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(54) **METHOD FOR DEPLETING OR ISOLATING A MOLECULE FROM A SOLUTION**

VERFAHREN ZUR ENTFERNUNG ODER ABTRENNUNG EINES MOLEKÜLS AUS EINER LÖSUNG

MÉTHODE POUR SÉPARER OU ISOLER UNE MOLECULE D'UNE SOLUTION

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Description

[0001] The present invention relates to a method of depleting a molecule from a solution according to claim 1 and a method of isolating a molecule from a solution according to claim 4.

FIELD AND BACKGROUND OF THE INVENTION

[0002] In nature there is an enormous variety of enzymes that catalyze reactions, some of which have industrial use. These include oxidoreductases, transferases, hydrolases, lyases, isomerases, and ligases. Immobilization of enzymes on solid substrates sometimes offers advantages over the use of a free enzyme. For example, immobilization can stabilize enzymes, enable better control of enzymatic reactions, allow the reuse of the enzyme and prevent enzyme loss with time. The material bearing the immobilized enzyme has a significant role in evoking these advantages both from architectural and chemical points of view.

[0003] Nanofibers and polymeric nanofibers in particular can be produced by an electrospinning process (Reneker DH., et al., 2006; Ramakrishna S., et al., 2005; Li D., et al., 2004; PCT WO 2006/106506 to the present inventors). Electrospun polymeric nanofibers have been widely used in biological applications such as scaffolds, carriers for biologically active molecules like proteins and enzymes (Xie J., et al., 2003; Zhang YZ., et al., 2006; Jiang H., et al., 2006; and Patel AC., et al., 2006) and encapsulation of viruses and bacteria (Salalha W., et al., 2006).

[0004] Several approaches can be used to entrap or attach enzymes to electrospun fibers. One approach is to immobilize the enzyme on the outer surface of the nanofibers by either covalently attaching the desired enzyme to the functional groups of the polymer surface (Ye P., et al., 2006; Jia H., et al., 2002; Kim TG., et al., 2006) or physically absorbing the enzyme to the surface (Huang XJ., et al., 2006). The second approach, which results in encapsulation of enzymes, is based on mixing the enzyme with the polymer solution prior to the electrospinning process (Xie J. and Hsieh Y-L, 2003). However, encapsulation is often associated with leaching of the enzymes, e.g., via fiber dissolution and burst releases (Zhang YZ., et al., 2006), especially, when the host polymer is a water soluble polymer such as poly(vinyl alcohol) (PVA) or dextran. To prevent immediate dissolution of the fibers in a physiological environment (e.g., blood) and the subsequent enzyme leaching, the electrospun fibers can be crosslinked by chemical or physical agents such as glutaraldehyde or UV irradiation. Alternatively, Zeng J, et al. (2005) suggested that PVA fibers can be coated with water insoluble polymers using a chemical vapor deposition (CVD). However, the organic solvents of the water insoluble polymers are harmful to biological material and can lead to loss of enzymatic activity. To overcome this problem, Herricks et al. (2005) suggested to use surfactant-stabilized enzymes in an organic solution of polystyrene (PS) as a spinning solution. In this way the electrospun nanofibers are insoluble in water and the enzymatic activity is retained due to surfactant stabilization (Herricks TE., et al., 2005).

[0005] Sun and co-workers (Sun Z, et al., 2003) describe the production of core-shell nanofibers (*i.e.*, filled fibers) by co-electrospinning of two polymeric solutions using a two co-axial capillaries spinneret. US patent application No. 20060119015 to Wehrspohn R., et al. describes the production of hollow fibers by introducing a liquid containing a polymer to a porous template material, and removal of the template following polymer solidification. PCT/IB2007/054001 to the present inventors discloses methods of producing electrospun microtubes (*i.e.*, hollow fibers) which can be further filled with liquids and be used as microfluidics.

[0006] Dror Y., et al. 2007 (Small, 3(6): 1064-1073) describe one-step production of polymeric microtubes by co-electrospinning with an incorporated green fluorescent protein (GFP). The method of depleting a molecule from a solution of the present invention is defined in claim 1 and the method of isolating a molecule from a solution of the present invention is defined in claim 4.

[0007] A method used for producing the microtubes used in the present invention comprises: co-electrospinning two polymeric solutions through co-axial capillaries, wherein a first polymeric solution of the two polymeric solutions is for forming a shell of the microtube and a second polymeric solution of the two polymeric solutions is for forming a coat over an internal surface of the shell, the first polymeric solution is selected solidifying faster than the second polymeric solution and a solvent of the second polymeric solution is selected incapable of dissolving the first polymeric solution and wherein the second polymeric solution comprises the molecule-of-interest, thereby attaching the molecule-of-interest to the microtube.

[0008] A microtube comprising an electrospun shell, an electrospun coat over an internal surface of the shell and a molecule-of-interest attached to the microtube is used in the present invention.

[0009] According to an aspect of some embodiments of the present invention there is provided a method of depleting a molecule from a solution, comprising contacting the solution with said microtube, wherein the member of the affinity pair is selected capable of binding the molecule, thereby depleting the molecule from the solution.

[0010] According to an aspect of some embodiments of the present invention there is provided a method of isolating a molecule from a solution, comprising: (a) contacting the solution with said microtube under conditions which allow binding of the molecule to the microtube via the member of the affinity pair which is selected capable of binding the

molecule, and; (b) eluting the molecule from the microtube; thereby isolating the molecule from the solution.

[0011] According to some embodiments of the invention, the electrospun shell is formed of a first polymeric solution and the electrospun coat is formed of a second polymeric solution.

[0012] According to some embodiments of the invention, the first polymeric solution solidifies faster than the second polymeric solution.

[0013] According to some embodiments of the invention, a solvent of the second polymeric solution is incapable of dissolving the first polymeric solution.

[0014] According to some embodiments of the invention, the electrospun shell comprises a polymer selected from the group consisting of poly (ε-caprolactone) (PCL), polyamide, poly(siloxane), poly(silicone), poly(ethylene), poly(vinyl pyrrolidone), poly(2-hydroxy ethylmethacrylate), poly(N-vinyl pyrrolidone), poly(methyl methacrylate), poly(vinyl alcohol), poly(acrylic acid), poly(vinyl acetate), polyacrylamide, poly(ethylene-co-vinyl acetate), poly(ethylene glycol), poly(methacrylic acid), polylactide, polyglycolide, poly(lactide-coglycolide), polyanhydride, polyorthoester, poly(carbonate), poly(acrylonitrile), poly(ethylene oxide), polyaniline, polyvinyl carbazole, polystyrene, poly(vinyl phenol), polyhydroxyacid, poly(caprolactone), polyanhydride, polyhydroxyalkanoate, polyurethane, collagen, albumin, alginate, chitosan, starch, hyaluronic acid, and whereas the electrospun coat comprises a polymer selected from the group consisting of poly(acrylic acid), poly(vinyl acetate), polyacrylamide, poly(ethylene-co-vinyl acetate), poly(ethylene glycol), poly(methacrylic acid), polylactide polyglycolide, poly(lactide-coglycolide), polyanhydride, polyorthoester, poly(carbonate), poly(ethylene oxide), polyaniline, polyvinyl carbazole, polystyrene, poly(vinyl phenol), polyhydroxyacid, alginate, starch, hyaluronic acid.

[0015] According to some embodiments of the invention, a solvent of the first polymeric solution evaporates faster than a solvent of the second polymeric solution.

[0016] According to some embodiments of the invention, the electrospinning is effected using a rotating collector.

[0017] According to some embodiments of the invention, a solvent of the second polymeric solution is capable of evaporating through the internal surface of the shell.

[0018] According to some embodiments of the invention, the second polymeric solution is capable of wetting the internal surface of the shell.

[0019] According to some embodiments of the invention, a thickness of the shell is from about 100 nm to about 20 micrometer.

[0020] According to some embodiments of the invention, an internal diameter of the microtube is from about 50 nm to about 20 micrometer.

[0021] According to some embodiments of the invention, the first and the second polymeric solutions are selected from the group consisting of: 10 % poly (ε-caprolactone) (PCL) in chloroform (CHCl₃) and dimethylformamide (DMF) (80:20 by weight) as the first polymeric solution and 4 % poly(ethylene oxide) (PEO) in water (H₂O) and ethanol (60:40 by weight) as the second polymeric solution, 10 % PCL in CHCl₃ and DMF (80:20 by weight) as the first polymeric solution and 6 % PEO in H₂O and ethanol (60:40 by weight) as the second polymeric solution, 9 % PCL in CHCl₃ and DMF (90:10 by weight) as the first polymeric solution and 7 % PEO in H₂O as the second polymeric solution, 10 % PCL in CHCl₃ and DMF (80:20 by weight) as the first polymeric solution and 9 % poly(vinyl alcohol) (PVA) in water and ethanol (50:50 by weight) as the second polymeric solution, and 10 % PCL in CHCl₃ and DMF (90:10 by weight) as the first polymeric solution and 4 % (w/w) PEO in ethanol:H₂O (26:74 by weight) as a second polymeric solution.

[0022] According to some embodiments of the invention, the microtube is filled with a liquid.

[0023] According to some embodiments of the invention, the first and the second polymeric solutions are biocompatible.

[0024] According to some embodiments of the invention, the molecule-of-interest is attached to the coat over the internal surface of the shell.

[0025] According to some embodiments of the invention, the molecule-of-interest is attached to the shell of the microtube.

[0026] According to some embodiments of the invention, the molecule-of-interest comprises a polypeptide, a polynucleotide, a carbohydrate, a small molecule, or any combination thereof.

[0027] According to the invention, the molecule-of-interest is a member of an affinity pair.

[0028] According to some embodiments of the invention, the polypeptide is an enzyme.

[0029] According to some embodiments of the invention, the enzyme is alkaline phosphatase (SEQ ID NO: 1 or 8) or beta-galactosidase (SEQ ID NO:2 or 9).

[0030] According to some embodiments of the invention, the first polymeric solution comprises polyethylene glycol (PEG).

[0031] According to some embodiments of the invention, the shell comprises pores.

[0032] According to some embodiments of the invention, the shell prevents diffusion of the molecule-of-interest there-through.

[0033] According to some embodiments of the invention, the substrate-of-interest comprises incorporating the substrate-of-interest in a synthesis reaction catalyzed by the molecule-of-interest.

[0034] According to some embodiments of the invention, the substrate-of-interest comprises incorporating the sub-

strate-of-interest in a catabolism reaction catalyzed by the molecule-of-interest.

[0035] According to some embodiments of the invention, the method further comprising collecting the solution following the contacting.

[0036] According to some embodiments of the invention, the solution comprises blood.

[0037] According to some embodiments of the invention, the affinity pair is selected from the group consisting of an enzyme and a substrate, a hormone and a receptor, an antibody and an antigen, a polypeptide and a polynucleotide, a polynucleotide and a cognate polynucleotide, a polypeptide and a metal ion, a polypeptide and a carbohydrate.

[0038] According to some embodiments of the invention, a therapeutically effective amount of the molecule-of-interest is capable of treating a pathology in the subject.

[0039] According to some embodiments of the invention, the molecule-of-interest comprises a polypeptide, and whereas a therapeutically effective amount of the polypeptide is capable of treating a pathology in the subject.

[0040] According to some embodiments of the invention, the pathology is selected from the group consisting of a metabolic disorder, an endocrine disease, an autoimmune disease, and cancer.

[0041] According to some embodiments of the invention, the polypeptide is selected from the group consisting of insulin (SEQ ID NO:6), phenylalanine hydroxylase (PAH) (SEQ ID NO:3), dystrophin (SEQ ID NO:4), beta-glucosidase (GBA) (SEQ ID NO:5), and ceruloplasmin ferroxidase (CP) (SEQ ID NO:7).

[0042] Unless otherwise defined, all technical and/or scientific terms used herein have the same meaning as commonly understood by one of ordinary skill in the art to which the invention pertains. Although methods and materials similar or equivalent to those described herein can be used in the practice or testing of embodiments of the invention, exemplary methods and/or materials are described below. In case of conflict, the patent specification, including definitions, will control. In addition, the materials, methods, and examples are illustrative only and are not intended to be necessarily limiting.

BRIEF DESCRIPTION OF THE DRAWINGS

[0043] Some embodiments of the invention are herein described, by way of example only, with reference to the accompanying drawings. With specific reference now to the drawings in detail, it is stressed that the particulars shown are by way of example and for purposes of illustrative discussion of embodiments of the invention. In this regard, the description taken with the drawings makes apparent to those skilled in the art how embodiments of the invention may be practiced.

[0044] In the drawings:

FIGs. 1A-D are images depicting high resolution scanning electron microscope (HRSEM) micrographs of (a) Type 1 fibers with alkaline phosphatase (AP); (b) Type 2 fibers with AP; (c) Type 1 fibers with beta-galactosidase (β -GAL); and (d) Type 2 fibers with β -GAL;

FIGs. 2A-C are graphs (Figures 2a-b) and a picture (Figure 2C) depicting the progress of the AP reactions with time for enzymes attached to (e.g., encapsulated within) the electrospun fibers and the free enzyme in the solution forming the coat over the internal surface of the shell (also referred to herein as a core solution) prior to the electrospinning. Figure 2A - the progress of the alkaline phosphatase reaction over 2500 minutes; Figure 2B - inset, the progress of the reaction through over the first 300 minutes; Note that the enzymatic reaction of the enzyme encapsulated within type 2 electrospun microtubes is faster than that of enzyme encapsulated within type 1 electrospun microtubes. Figure 2C - a photograph of a piece of mat (Type 1) immersed in the assay solution. The presence of the yellow reaction product, p-nitrophenol, is apparent; the reaction substrate was para-nitrophenyl phosphate;

FIG. 3 is a histogram depicting the relative activity of AP enzyme for different types of fibers (type 1 and type 2) and in dwelling buffers. Mat = the electrospun fibers (microtubes) with the attached (encapsulated) enzymes; rinsing buffer = the buffer used to only rinse the fibers, without any additional incubation time; 24 hrs. buffer = the buffer following incubation of the fibers therein for 24 hours; 72 hrs. buffer = the buffer following incubation of the fibers therein for 72 hours; core solution = the enzyme in the core solution prior to the electrospinning process.

FIGs. 4A-B are graphs depicting the progress of the β -GAL reactions with time for the two types of electrospun fibers and the free enzyme in the core solution. The substrate was ortho-nitrophenyl galactoside. Figure 4A - the progress of the β -GAL reactions over 5000 minutes as measured by the amount of ortho-nitrophenol generated; Figure 4B - inset of the graph of Figure 4a, the progress of the β -GAL reactions over the first 50 minutes;

FIG. 5 is a graph depicting the β -GAL reaction versus time for the mat and buffers for Type 2 fibers;

FIG. 6 is a histogram depicting the relative activity of the β -GAL and AP for different types of fibers;

FIGs. 7A-B are fluorescence microscope micrographs depicting Type 1 fibers with AP (Figure 7A) and β -GAL (Figure 7B). Size bars: 100 μ m (Figure 7A) and 50 μ m (Figure 7B).

FIG. 8 is a schematic illustration depicting the desorption process of the molecule-of-interest from the microtube of the invention. The molecule-of-interest (e.g., a protein, an enzyme) is attached to the coat over the internal surface

of the shell. Following contacting the microtube with a solution, the solution enters the microtube via the pores (an exemplary pore is marked by arrow No. 3) by a capillary rise (see arrow No. 1) and gradually wets and fills the microtube inner volume. The desorption of the molecule-of-interest from the internal surface of the microtube shell (which depends mainly on the rate of the release of the molecule-of-interest from the polymer) is shown by arrow No. 2. FIG. 9 depicts a multi-step enzymatic reaction performed using encapsulated molecules-of-interest (enzymes 1-4). Enzyme 1 (enz1) catalyzes the conversion of compound A to B; Enzyme 2 (enz2) catalyzes the conversion of compound B to C; Enzyme 3 (enz3) catalyzes the conversion of compound C to D; Enzyme 4 (enz4) catalyzes the conversion of compound D to E.

FIG. 10 is a schematic presentation depicting Atrazine degradation by the isolated *Pseudomonas* ADP enzymes: AtzA (atrazine chlorohydrolase, e.g., GenBank Accession No. NP_862474), AtzB (hydroxyatrazine hydrolase, e.g., GenBank Accession No. NP_862481), AtzC (N-isopropylammelide isopropylamino hydrolase, e.g., GenBank Accession No. NP_862508), AtzD (cyanuric acid amidohydrolase, e.g., GenBank Accession No. NP_862537), AtzE (biuret hydrolase, e.g., GenBank Accession No. NP_862538) and AtzF (allophanate hydrolase, e.g., GenBank Accession No. AAK50333) which are attached to the microtube of the invention.

DESCRIPTION OF SPECIFIC EMBODIMENTS OF THE INVENTION

[0045] Before explaining at least one embodiment of the invention in detail, it is to be understood that the invention is not necessarily limited in its application to the details set forth in the following description or exemplified by the Examples. The invention is capable of other embodiments or of being practiced or carried out in various ways.

[0046] While reducing the invention to practice, the present inventors have uncovered that a member of an affinity pair can be attached to electrospun microtubes. Thus, as is shown in Figures 1a-b and described in Example 1 of the Examples section which follows, Two types of electrospun microtubes containing member of an affinity pair were formed: Type 1 microtubes which exhibit a non-porous shell, and Type 2 microtubes which exhibit a porous shell due to the presence of PEG in the polymeric solution forming the shell. The enzymatic activity contained within the microtubes was at the same order of magnitude as that of the polymeric solution prior to the electrospinning process (Figures 2a-b, 3, 4a-b and 6; Examples 1-3 of the Examples section which follows) indicating that surprisingly the process of production did not compromise the functionality of the delicate protein material incorporated into the tube. In addition, as is shown in Figure 3 and described in Example 2 of the Examples section which follows, both the porous and non-porous microtubes were capable of releasing enzymes attached thereto. Moreover, during the electrospinning process, some of the alkaline phosphatase enzyme migrated to the outer surface of the microtube shell and was released therefrom into the aqueous environment (Figure 3, Example 2), while the β -GAL enzyme remained within the internal surface of the shell (Figure 5, Example 3). In addition, as is further described in Example 3 of the Examples section which follows, the activity of the enzymes attached to the internal surface of the shell was increased in the presence of a porous shell which enabled the passage of substrates therethrough (Figures 4a-b). These results support the use of the microtubes of the invention as micro-reactors (e.g., bioreactors) for various synthesis, hydrolysis, isolation and purification reactions.

[0047] The method for producing microtubes useful in the present invention is effected by co-electrospinning two polymeric solutions through co-axial capillaries, wherein a first polymeric solution of the two polymeric solutions is for forming a shell of the microtube and a second polymeric solution of the two polymeric solutions is for forming a coat over an internal surface of the shell, the first polymeric solution is selected solidifying faster than the second polymeric solution and a solvent of the second polymeric solution is selected incapable of dissolving the first polymeric solution and wherein the second polymeric solution comprises the molecule-of-interest, thereby attaching the molecule-of-interest to the microtube.

[0048] As used herein the term "microtube" refers to a hollow tube having an inner diameter of e.g., about 200 nm to about 50 μ m and an outer diameter of e.g., about 0.5 μ m to about 100 μ m.

[0049] According to some embodiments of the invention the thickness of the microtube shell can vary from a few nanometers to several micrometers, such as from about 100 nm to about 20 μ m, e.g., from about 200 nm to about 10 μ m, from about 100 nm to about 5 μ m, from about 100 nm to about 1 μ m, e.g., about 500 nm.

[0050] According to some embodiments of the invention the internal diameter of the microtube shell can vary from a few nanometers to several micrometers, such as from about 50 nm to about 50 μ m, e.g., from about 100 nm to about 20 μ m, from about 200 nm to about 10 μ m, from about 500 nm to about 5 μ m, from about 1 μ m to about 5 μ m, e.g., about 3 μ m.

[0051] According to some embodiments of the invention, the microtube may have a length which is from about 0.1 millimeter (mm) to about 20 centimeter (cm), e.g., from about 1-20 cm, e.g., from about 5-10 cm.

[0052] As used herein the term "attaching" refers to the binding of the molecule-of-interest to the polymer(s) comprised in the microtube of the invention via covalent or non-covalent binding (e.g., via an electrostatic bond, a hydrogen bond, a van-Der Waals interaction) so as to obtain an absorbed, embedded or immobilized molecule-of-interest to the microtube of the invention.

[0053] According to some embodiments of the invention, the length (L) of the microtube can be several orders of magnitude higher (e.g., 10 times, 100 times, 1000 times, 10,000 times) than the microtube's diameter (D). Accordingly, a molecule-of-interest which is attached to such a microtube is referred to as being entrapped or encapsulated within the microtube.

5 **[0054]** According to some embodiments of the invention, covalent attachment of the molecule-of-interest can be via functional groups such as SH groups, amino groups, carboxyl groups which are added to the polymer(s) forming the microtube.

10 **[0055]** As used herein the phrase "co-electrospinning" refers to a process in which at least two polymeric solutions are electrospun from co-axial capillaries (i.e., at least two capillary dispensers wherein one capillary is placed within the other capillary while sharing a co-axial orientation) forming the spinneret within an electrostatic field in a direction of a collector. The capillary can be, for example, a syringe with a metal needle or a bath provided with one or more capillary apertures from which the polymeric solution can be extruded, e.g., under the action of hydrostatic pressure, mechanical pressure, air pressure and high voltage.

15 **[0056]** The collector serves for collecting the electrospun element (e.g., the electrospun microtube) thereupon. Such a collector can be a rotating collector or a static (non rotating) collector. When a rotating collector is used, such a collector may have a cylindrical shape (e.g., a drum), however, the rotating collector can be also of a planar geometry (e.g., an horizontal disk). The spinneret is typically connected to a source of high voltage, such as of positive polarity, while the collector is grounded, thus forming an electrostatic field between the dispensing capillary (dispenser) and the collector. Alternatively, the spinneret can be grounded while the collector is connected to a source of high voltage, such as with negative polarity. As will be appreciated by one ordinarily skilled in the art, any of the above configurations establishes motion of a positively charged jet from the spinneret to the collector. Reverse polarity for establishing motions of a negatively charged jet from the spinneret to the collector are also contemplated.

20 **[0057]** For electrospinning, the first polymeric solution is injected into the outer capillary of the co-axial capillaries while the second polymeric solution is injected into the inner capillary of the co-axial capillaries. In order to form a microtube (i.e., a hollow structure, as mentioned above), the first polymeric solution (which is for forming the shell of the microtube) solidifies faster than the second polymeric solution (also referred herein as a core polymeric solution, and is for forming a coat over the internal surface of the shell). In addition, the formation of a microtube also requires that the solvent of the second polymeric solution be incapable of dissolving the first polymeric solution.

25 **[0058]** The solidification rates of the first and second polymeric solutions are critical for forming the microtube. For example, for a microtube of about 100 μm , the solidification of the first polymer (of the first polymeric solution) can be within about 30 milliseconds (ms) while the solidification of the second polymer (of the second polymeric solution) can be within about 10-20 seconds. The solidification may be a result of polymerization rate and/or evaporation rate.

30 **[0059]** According to some embodiments of the invention; the solvent of the first polymeric solution evaporates faster than the solvent of second polymeric solution (e.g., the solvent of the first polymeric solution exhibits a higher vapor pressure than the solvent of the second polymeric solution).

35 **[0060]** According to some embodiments of the invention, the rate of evaporation of the solvent of the first polymeric solution is at least about 10 times faster than that of the solvent of the second polymeric solution. The evaporation rate of the solvent of the first polymeric solution can be at least about 100 times faster or at least about 1000 times faster than the evaporation rate of the solvent of second polymeric solution. For example, the evaporation of chloroform is significantly faster than the evaporation of an aqueous solution (water) due to the high vapor pressure at room temperature of the chloroform (195 mmHg) vs. that of the aqueous solution (23.8 mmHg).

40 **[0061]** When selecting a solvent of the second polymeric solution which is incapable of dissolving the first polymeric solution (i.e., a non-solvent of the first polymeric solution), the polymer of the first polymeric solution can solidify (e.g., through precipitation) and form a strong microtube shell which does not collapse, and is characterized by an even thickness. According to some embodiments of the invention, the first polymeric solution (e.g., the solvent of the first polymer) is substantially immiscible in the solvent of the second polymeric solution.

45 **[0062]** The solvent of the second polymeric solution may evaporate while the polymer (of the second polymeric solution) forms a thin layer on the internal surface of the shell.

50 **[0063]** According to some embodiments of the invention, the solvent of the second polymeric solution is capable of evaporating through the internal surface of the shell.

[0064] The flow rates of the first and second polymeric solutions can determine the microtube outer and inner diameter and thickness of shell. Non-limiting examples of microtubes generated by electrospinning using different flow rates are shown in Table 1 hereinbelow.

Table 1

Effect of the flow rates of the two polymeric solutions during electrospinning on microtube diameter and thickness of shell						
System No.	System: First polymeric solution/ Second polymeric solution	Flow rates (ml/hr)	R OuterFiber (μm)	d Shell thickness (μm)	V Voltage (kV)	Electrostatic field kV/cm
M5	First polymeric solution	4	3.0-4.5	0.5 \pm 0.1	8.5	0.43
	Second polymeric solution	0.5				
M10	First polymeric solution	10	2.3-4.0	1.0 \pm 0.1	8	0.5
	Second polymeric solution	0.3				
M11	First polymeric solution	10	3-6	1.0 \pm 0.1	9	0.56
	Second polymeric solution	2				

Table 1: Electrospinning was performed with the following solutions: First polymeric solution (for forming the shell) was 10 % PCL in CHCl₃/DMF (8:2 weight/weight); Second polymeric solution (for forming the coat) was 4 % PEO in H₂O/EtOH (6:4, weight/weight). PCL used was PCL 80 K; PEO used was PEO 600 K. The temperature during electrospinning was 22-26 °C. The relative humidity during electrospinning was 58 %, 52 % and 53 % for systems M5, M10 and M11, respectively. The flow rates were measured in milliliter per hour (ml/hr); the outer microtube radius (R) and the shell thickness (d) were measured in microns (μm). The voltage was measured in kilo volt (kV), and the electrostatic field was measured in kV per centimeter (cm). The resulting tubes were hollow (good tubes in systems M5 and M11, and mostly good in system M10).

[0065] As used herein the phrase "polymeric solution" refers to a soluble polymer, *i.e.*, a liquid medium containing one or more polymers, co-polymers or blends of polymers dissolved in a solvent. The polymer used by the invention can be a natural, synthetic, biocompatible and/or biodegradable polymer.

[0066] The phrase "synthetic polymer" refers to polymers that are not found in nature, even if the polymers are made from naturally occurring biomaterials. Examples include, but are not limited to, aliphatic polyesters, poly(amino acids), copoly(ether-esters), polyalkylenes oxalates, polyamides, tyrosine derived polycarbonates, poly(iminocarbonates), polyorthoesters, polyoxaesters, polyamidoesters, polyoxaesters containing amine groups, poly(anhydrides), polyphosphazenes, and combinations thereof.

[0067] Suitable synthetic polymers for use by the invention can also include biosynthetic polymers based on sequences found in naturally occurring proteins such as those of collagen, elastin, thrombin, fibronectin, or derivatives thereof or, starches, poly(amino acids), poly(propylene fumarate), gelatin, alginate, pectin, fibrin, oxidized cellulose, chitin, chitosan, tropoelastin, hyaluronic acid, polyethylene, polyethylene terephthalate, poly(tetrafluoroethylene), polycarbonate, polypropylene and poly(vinyl alcohol), ribonucleic acids, deoxyribonucleic acids, polypeptides, proteins, polysaccharides, polynucleotides and combinations thereof.

[0068] The phrase "natural polymer" refers to polymers that are naturally occurring. Non-limiting examples of such polymers include, silk, collagen-based materials, chitosan, hyaluronic acid, albumin, fibrinogen, and alginate.

[0069] As used herein, the phrase "co-polymer" refers to a polymer of at least two chemically distinct monomers. Non-limiting examples of co-polymers include, polylactic acid (PLA)-polyethyleneglycol (PEG), polyethylene glycol terephthalate (PET) / polybutylene terephthalate (PBT), PLA-polyglycolic acid (PGA), PEG-polycaprolactone (PCL) and PCL-PLA.

[0070] As used herein, the phrase "blends of polymers" refers to the result of mixing two or more polymers together

to create a new material with different physical properties.

[0071] The phrase "biocompatible polymer" refers to any polymer (synthetic or natural) which when in contact with cells, tissues or body fluid of an organism does not induce adverse effects such as immunological reactions and/or rejections, cellular death and the like. It will be appreciated that a biocompatible polymer can also be a biodegradable polymer.

[0072] According to some embodiments of the invention, the first and the second polymeric solutions are biocompatible.

[0073] Non-limiting examples of biocompatible polymers include polyesters (PE), PCL, Calcium sulfate, PLA, PGA, PEG, polyvinyl alcohol, polyvinyl pyrrolidone, Polytetrafluoroethylene (PTFE, teflon), polypropylene (PP), polyvinylchloride (PVC), Polymethylmethacrylate (PMMA), polyamides, segmented polyurethane, polycarbonate-urethane and thermoplastic polyether urethane, silicone-polyether-urethane, silicone-polycarbonate-urethane collagen, PEG-DMA, alginate, hydroxyapatite and chitosan, blends and copolymers thereof.

[0074] The phrase "biodegradable polymer" refers to a synthetic or natural polymer which can be degraded (*i.e.*, broken down) in the physiological environment such as by proteases or other enzymes produced by living organisms such as bacteria, fungi, plants and animals. Biodegradability depends on the availability of degradation substrates (*i.e.*, biological materials or portion thereof which are part of the polymer), the presence of biodegrading materials (e.g., microorganisms, enzymes, proteins) and the availability of oxygen (for aerobic organisms, microorganisms or portions thereof), lack of oxygen (for anaerobic organisms, microorganisms or portions thereof) and/or other nutrients. Examples of biodegradable polymers/materials include, but are not limited to, collagen (e.g., Collagen I or IV), fibrin, hyaluronic acid, polylactic acid (PLA), polyglycolic acid (PGA), polycaprolactone (PCL), polydioxanone (PDO), trimethylene carbonate (TMC), polyethyleneglycol (PEG), collagen, PEG-DMA, alginate, chitosan copolymers or mixtures thereof.

[0075] According to some embodiments, the polymeric solution can be made of one or more polymers, each can be a polymer or a co-polymer such as described hereinabove.

[0076] According to some embodiments of the invention, the polymeric solution of the invention is a mixture of at least one biocompatible polymer and a co-polymer (either biodegradable or non-biodegradable).

[0077] According to some embodiments of the invention, the first polymeric solution for forming the shell can be made of a polymer such as poly (ε-caprolactone) (PCL), polyamide, poly(siloxane), poly(silicone), poly(ethylene), poly(vinyl pyrrolidone), poly(2-hydroxy ethylmethacrylate), poly(N-vinyl pyrrolidone), poly(methyl methacrylate), poly(vinyl alcohol), poly(acrylic acid), poly(vinyl acetate), polyacrylamide, poly(ethylene-co-vinyl acetate), poly(ethylene glycol), poly(methacrylic acid), polylactide, polyglycolide, poly(lactide-coglycolide), polyanhydride, polyorthoester, poly(carbonate), poly(acrylonitrile), poly(ethylene oxide), polyaniline, polyvinyl carbazole, polystyrene, poly(vinyl phenol), polyhydroxyacid, poly(caprolactone), polyanhydride, polyhydroxyalkanoate, polyurethane, collagen, albumin, alginate, chitosan, starch, hyaluronic acid, and blends and copolymers thereof.

[0078] According to some embodiments of the invention, the second polymeric solution for forming the coat over the internal surface of the shell can be made of a polymer such as poly(acrylic acid), poly(vinyl acetate), polyacrylamide, poly(ethylene-co-vinyl acetate), poly(ethylene glycol), poly(methacrylic acid), polylactide, polyglycolide, poly(lactide-coglycolide), polyanhydride, polyorthoester, poly(carbonate), poly(ethylene oxide), polyaniline, polyvinyl carbazole, polystyrene, poly(vinyl phenol), polyhydroxyacid, alginate, starch, hyaluronic acid, and blends and copolymers thereof.

[0079] During the formation of the microtube shell (e.g., following the solidification of the first polymeric solution) the second polymeric solution flows within the internal surface of the shell.

[0080] According to some embodiments of the invention, the second polymeric solution is selected capable of wetting the internal surface of the shell.

[0081] Various polymeric solutions which are known in the art as capable of wetting other polymeric surfaces (for forming the shell) can be used. Following is a non-limiting list of pairs of polymeric solutions in which the second polymeric solution is capable of wetting the internal surface of the shell formed by the first polymeric solution.

Table 2

Pairs of polymeric solutions for producing the microtube of the invention	
First polymeric solution forming the shell	Second polymeric solution capable of wetting the internal surface of the shell
10 % poly (ε-caprolactone) (PCL); in chloroform (CHCl ₃) and dimethylformamide (DMF) (80:20 by weight)	4 % poly(ethylene oxide) (PEO); in water (H ₂ O) and ethanol (60:40 by weight)
Nylon 6,6 in formic acid 7 to 12 wt %	4 % poly(ethylene oxide) (PEO); in water (H ₂ O) and ethanol (60:40 by weight)

(continued)

Pairs of polymeric solutions for producing the microtube of the invention	
First polymeric solution forming the shell	Second polymeric solution capable of wetting the internal surface of the shell
Poly(L-lactide-co-glycolide) (PLGA 10:90) in hexafluoroisopropanol (HFIP) concentrations ranging from 2 to 7 weight % solution.	4 % poly(ethylene oxide) (PEO) in water (H ₂ O) and ethanol (60:40 by weight)
Poly(L-lactide-co-glycolide) (PLGA 15:85) hexafluoroisopropanol (HFIP) concentrations ranging from 2 to 7 weight% solution.	4 % poly(ethylene oxide) (PEO); in water (H ₂ O) and ethanol (60:40 by weight)
poly(lactide-co-glycolide) (PLGA; 1-lactide/glycolide_50/50) 1,1,1,3,3,3-hexafluoro-2-propanol (HFIP) concentrations ranging from 2 to 7 weight% solution.	4 % poly(ethylene oxide) (PEO); in water (H ₂ O) and ethanol (60:40 by weight)
polyglycolide (PGA) in chloroform 3-10 weight % solution.	9 % poly(vinyl alcohol) (PVA); in water and ethanol (50:50 by weight)
poly(L-lactide) (PLA) in chloroform 3-10 weight % solution.	9 % poly(vinyl alcohol) (PVA); in water and ethanol (50:50 by weight)
Segmented polyurethane in DMF and THF (80:20 by weight)	9 % poly(vinyl alcohol) (PVA); in water and ethanol (50:50 by weight)
Polyurethane in DMF and tetrahydrofuran, THF (80:20 by weight)	9 % poly(vinyl alcohol) (PVA); in water and ethanol (50:50 by weight)
PLGA (poly lactic-co-glycolic acid); in chloroform and DMSO (dimethyl sulfoxide) in chloroform and DMSO (80:20 by weight).	9 % poly(vinyl alcohol) (PVA); in water and ethanol (50:50 by weight)
10 % PCL in CHCl ₃ / DMF (80:20 by weight)	6 % PEO in H ₂ O / EtOH (60:40 by weight)
9 % PCL in CHCl ₃ / DMSO (90:10 by weight)	7 % PEO in H ₂ O
10 % PCL in CHCl ₃ / DMF (80:20 by weight)	9 % PVA in ethanol/water (50:50 by weight)
10 % PCL 80 K CHCl ₃ :DMF (90:10 by weight)	4 % (w/w) PEO 600 K; in ethanol:H ₂ O (26:74 by weight)
10 % PCL 80 K + 1 % PEG 6 K CHCl ₃ :DMF (90:10 by weight)	4 % (w/w) PEO 600 K; in ethanol:H ₂ O (26:74 by weight)
Table 2 (cont.). The polymers forming the solutions and the solvents are provided by weight ratios, <i>i.e.</i> , a weight/weight (w/w) ratio.	

[0082] According to some embodiments of the invention, the first and the second polymeric solutions are selected from the group consisting of: 10 % poly (ε-caprolactone) (PCL) in chloroform (CHCl₃) and dimethylformamide (DMF) (80:20 by weight) as the first polymeric solution and 4 % poly(ethylene oxide) (PEO) in water (H₂O) and ethanol (60:40 by weight) as the second polymeric solution, 10 % PCL in CHCl₃ and DMF (80:20 by weight) as the first polymeric solution and 6 % PEO in water and ethanol (60:40 by weight) as the second polymeric solution, 9 % PCL in CHCl₃ and DMF (90:10 by weight) as the first polymeric solution and 7 % PEO in water as the second polymeric solution, 10 % PCL in CHCl₃ and DMF (80:20 by weight) as the first polymeric solution and 9 % poly(vinyl alcohol) (PVA) in water and ethanol (50:50 by weight) as the second polymeric solution and 10 % PCL in CHCl₃ and DMF (90:10 by weight) as the first polymeric solution and 4 % (w/w) PEO in ethanol:H₂O (26:74 by weight) as a second polymeric solution.

[0083] To enable a flow of a liquid-of-interest within the microtube, *i.e.*, along the coat polymer covering the internal surface of the shell (which originates from the second polymer solution), the surface (thin film) formed by the coat polymer should be designed such that it can be wetted by the liquid-of-interest. The ability to wet (wettability) polymer films by liquids is known in the art. For example, silicone oil or water can wet a surface made of a PEO polymer. It will be appreciated that the wettability of the coat polymer covering the internal surface of the shell can be controlled (e.g., improved) for example by attaching functional groups such as hydroxyl groups (OH) which increase the hydrophilicity

of the coat by a plasma treatment [see Thurston RM, Clay JD, Schulte MD, Effect of atmospheric plasma treatment on polymer surface energy and adhesion, Journal of Plastic Film & Sheeting 23 (1): 63-78 JAN 2007.

[0084] As is further discussed hereinabove and in the Examples section which follows, for certain applications the microtube shell may comprise pores, thus creating a "breathing" tube. Methods of forming "breathing" microtube (*i.e.*, microtubes with pores in the shell thereof) are described in PCT/IB2007/054001 to the present inventors. Briefly, "breathing" tubes can be formed by the inclusion of a high percent (e.g., at least 80 %) of a volatile component such as tetrahydrofuran (THF), chloroform, acetone, or trifluoroethanol (TFE) in the first polymeric solution forming the shell, and/or by the inclusion of a water-soluble polymer such as polyethylene glycol (PEG) in the first polymeric solution forming the shell so that the first polymeric solution comprises a blend of polymers in which one is water-soluble and the other is water-insoluble (e.g., a blend of PEG and PCL). Alternatively, "breathing" microtubes can be formed by inducing pores in the shell after the completion of the electrospinning process, essentially as described in PCT WO 2006/106506 to the present inventors, such as by passing an electrical spark or a heated puncturing element through the electrospun shell, or by using a pulsed or continuous laser beam through the electrospun shell.

[0085] According to some embodiments of the invention, the first polymeric solution comprises PEG for inducing pores in the shell. For example, to generate pores greater (>) than 150 nm in diameter, the first polymeric solution may include about 4 % PEG MW 35 kDa. Similarly, to generate pores smaller (<) than 150 nm in diameter, the first polymeric solution may include about 2 % PEG MW 6 kDa.

[0086] The microtube shell of the invention can be designed such that it enables the passage of certain molecules (e.g., a substrate of an enzyme) while preventing the passage of other molecules (e.g., a certain enzyme), depending on the geometry (pore size) and/or the electrical charge of the molecules with respect to the geometry (length and radius), surface energy, electrical charge of the nanopore(s) of the shell, and the viscosity and surface tension of the liquid containing the molecules (e.g., the substrate of the enzyme). In addition, the porosity and pore size of the shell can control the release of the molecule-of-interest which is attached to the microtube. For example, a higher porosity and/or pore size can result in increased rate of release of the molecule-of-interest.

[0087] Alternatively, the microtube shell can be made such that it prevents diffusion or any passage of the molecule-of-interest therethrough (*i.e.*, substantially devoid of pores, or with pores smaller than the molecule-of-interest).

[0088] As mentioned, the second polymeric solution comprises the molecule-of-interest. Such a molecule (or molecules) can be any naturally occurring or synthetic molecule such as a polypeptide, a polynucleotide, a carbohydrate or a polysaccharide, a lipid, a drug molecule, a small molecule (e.g., a nucleotide base, an amino acid, a nucleotide, an antibiotic, a vitamin or a molecule which is smaller than 0.15 kDa), or any combination thereof. The molecule-of-interest can be produced by recombinant DNA technology or by known synthesis methods such as solid phase.

[0089] According to some embodiments of the invention, the molecule-of-interest comprises a polypeptide such as an enzyme. Such polypeptides (e.g., enzymes) can be naturally occurring (e.g., mammals such as primates, rodents and Homo sapiens, plants, fungi, protozoa, bacteria and viruses) or synthetic (e.g., derived from in vitro evolution) and can be selected according to the desired application.

[0090] The following non-limiting list of enzymes can be attached to the microtube of the invention: DNA polymerase (EC 2.7.7.7), DNase (EC 3.1.11.4), RNA polymerase (EC 2.7.7.6), DNA ligase (EC 6.5.1.1), RNA ligase (EC 6.5.1.3), alcohol dehydrogenase (EC 1.1.1.1), homoserine dehydrogenase (EC 1.1.1.3), acetoin dehydrogenase (EC 1.1.1.5), glycerol dehydrogenase (EC 1.1.1.6), L-xylulose reductase (EC 1.1.1.10), L-arabinitol 2-dehydrogenase (EC 1.1.1.13), L-iditol 2-dehydrogenase (EC 1.1.1.14), mannitol-1-phosphate 5-dehydrogenase (EC 1.1.1.17), mannitol 2-dehydrogenase (EC 1.1.1.138), glucose oxidase (EC 1.1.3.4), L-sorbose oxidase (EC 1.1.3.11), lactate-malate transhydrogenase (EC 1.1.99.7), formaldehyde dehydrogenase (EC 1.2.1.1), aryl-aldehyde dehydrogenase (EC 1.2.1.29), aldehyde oxidase (EC 1.2.3.1), pyruvate synthase (EC 1.2.7.1), cortisone α -reductase (EC 1.3.1.4), lathosterol oxidase (EC 1.3.3.2), D-proline reductase (EC 1.4.4.1), dihydrofolate reductase (EC 1.5.1.3), methylenetetrahydrofolate reductase (NADPH) (EC 1.5.1.20), cystine reductase (NADH) (EC 1.6.1.4), cob(II)alamin reductase (EC 1.6.99.9), sulfite reductase (EC 1.8.1.2), cytochrome-c oxidase (EC 1.9.3.1), NADH peroxidase (EC 1.11.1.1), homogentistate 1,2-dioxygenase (EC 1.13.11.5), *Photinus-luciferin* 4-monoxygenase (1.13.12.7), anthranilate 3-monoxygenase (EC 1.14.13.35), steroid 9 α -monoxygenase (EC 1.14.99.25), mercury(II) reductase (EC 1.16.1.1), nicotinamide N-methyltransferase (EC 2.1.1.1), thymidylate synthase (EC 2.1.1.45), site-specific DNA-methyltransferase (adenine-specific) (EC 2.1.1.72), tryptophan 2-C-methyltransferase (EC 2.1.1.106), glycine formiminotransferase (EC 2.1.2.4), aspartate carbamoyltransferase (EC 2.1.3.2), transaldolase (EC 2.2.1.2), arylamine N-acetyltransferase (EC 2.3.1.5), arginine N-succinyltransferase (EC 2.3.1.109), phosphorylase (EC 2.4.1.1), glycosaminoglycan galactosyltransferase (EC 2.4.1.74), thymidine phosphorylase (EC 2.4.2.4), β -galactoside α -2,6-sialyltransferase (EC 2.4.99.1), galactose-6-sulfurylase (EC 2.5.1.5), aspartate transaminase (2.6.1.1), hexokinase (EC 2.7.1.1), choline kinase (EC 2.7.1.32), acetate kinase (EC 2.7.2.1), creatine kinase (EC 2.7.3.2), adenylate kinase (EC 2.7.4.3), nucleotide pyrophosphokinase (EC 2.7.6.4), sulfate adenylyltransferase (ADP) (EC 2.7.7.5), aryl sulfotransferase (EC 2.8.2.1), carboxylesterase (3.1.1.1), acetyl-CoA hydrolase (EC 3.1.2.1), alkaline phosphatase (3.1.3.1), phosphodiesterase I (EC 3.1.4.1), dGTPase (EC 3.1.5.1), steryl-sulfatase (EC 3.1.6.2), exodeoxyribonuclease I (EC 3.1.11.1), ribonuclease T1 (EC 3.1.27.3), α -amylase (EC 3.2.1.1), purine

nucleosidase (EC 3.2.2.1), epoxide hydrolase (EC 3.3.2.3), lysyl aminopeptidase (EC 3.4.11.15), carboxypeptidase A2 (EC 3.4.17.15), trypsin (EC 3.4.21.4), glutaminase (EC 3.5.1.2), barbiturase (EC 3.5.2.1), ATP deaminase (EC 3.5.4.18), inorganic pyrophosphatase (EC 3.6.1.1), oxaloacetase (EC 3.7.1.1), oxalate decarboxylase (EC 4.1.1.2), mandelonitrile lyase (EC 4.1.2.10), isocitrate lyase (4.1.3.1), fumarate hydratase (EC 4.2.1.2), pectate lyase (EC 4.2.2.2), histidine ammonia-lyase (EC 4.3.1.3), cyanate lyase (4.3.99.1), cysteine lyase (EC 4.4.1.10), DDT-dehydrochlorinase (EC 4.5.1.1), adenylate cyclase (EC 4.6.1.1), alanine racemase (5.1.1.1), tartrate epimerase (EC 5.1.2.5), retinal isomerase (EC 5.2.1.3), L-rhamnose isomerase (EC 5.3.1.14), prostaglandin-D synthase (EC 5.3.99.2), phosphoglucomutase (EC 5.4.2.2), lanosterol synthase (EC 5.4.99.7), DNA topoisomerase (EC 5.99.1.2), tyrosine-tRNA ligase (EC 6.1.1.1), acetate-CoA ligase (EC 6.2.1.1), acetylcholinesterase (EC 3.1.1.7), butyrylcholinesterase (EC 3.1.1.8) and glutathione synthase (EC 6.3.2.3).

[0091] According to an embodiment of the invention, the enzyme which is attached to the microtube is alkaline phosphatase (e.g., SEQ ID NO:1 or 8; EC 3.1.3.1) or beta-galactosidase (e.g., SEQ ID NO:2 or 9; EC 3.2.1.23).

[0092] The term "polynucleotide" as used herein refers to a single stranded or double stranded oligomer or polymer of ribonucleic acid (RNA) or deoxyribonucleic acid (DNA) or mimetics thereof. This term includes polynucleotides composed of naturally-occurring bases, sugars and covalent internucleoside linkages (e.g., backbone) as well as polynucleotides having non-naturally-occurring portions which function similarly to respective naturally-occurring portions.

[0093] The polynucleotide which is attached to the microtube of the invention can be generated according to any oligonucleotide synthesis method known in the art such as enzymatic synthesis, liquid phase or solid phase synthesis (using a commercially available equipment from, for example, Applied Biosystems). Equipment and reagents for executing solid-phase synthesis are commercially available from, for example, Applied Biosystems. Any other means for such synthesis may also be employed; the actual synthesis of the oligonucleotides is well within the capabilities of one skilled in the art and can be accomplished via established methodologies as detailed in, for example, "Molecular Cloning: A laboratory Manual" Sambrook et al., (1989); "Current Protocols in Molecular Biology" Volumes I-III Ausubel, R. M., ed. (1994); Ausubel et al., "Current Protocols in Molecular Biology", John Wiley and Sons, Baltimore, Maryland (1989); Perbal, "A Practical Guide to Molecular Cloning", John Wiley & Sons, New York (1988) and "Oligonucleotide Synthesis" Gait, M. J., ed. (1984) utilizing solid phase chemistry, e.g. cyanoethyl phosphoramidite followed by deprotection, desalting and purification by for example, an automated trityl-on method or HPLC. Liquid phase synthesis of oligonucleotides can be performed using methods known in the art (see for example, Bonora GM, et al., 1998, Biol. Proced. Online. 1: 59-69; Padiya KJ and Salunkhe MM., 2000, Bioorg. Med. Chem. 8: 337-42). It will be appreciated that for the preparation of multiple labeled polynucleotides, a large scale oligonucleotide synthesis can be utilized essentially as described elsewhere (Anderson NG. et al., Appl Biochem Biotechnol. 1995 Jul-Sep;54(1-3):19-42; Rahmann S., Proc IEEE Comput Soc Bioinform Conf. 2002;1:54-63).

[0094] Additionally or alternatively, the polynucleotide which is attached to the microtube of the invention can be generated by recombinant DNA techniques using any known DNA replication or transcription system (e.g., using bacterial cells, eukaryotic cells).

[0095] As mentioned, the molecule-of-interest can be a drug molecule. Such a drug can be any synthetic, chemical or biological molecule.

[0096] Non-limiting examples of biological drug molecules include antisense oligonucleotides, Ribozymes, DNAzymes, siRNA, receptor agonists, antagonists, hormones, growth factors and antibodies. Non-limiting examples of which chemical drug molecules include chemotherapy agents, Paclitaxel (Taxol®), radiation seed particles (e.g., see Hypertext Transfer Protocol://World Wide Web (dot) oncura (dot) com), as well as natural or synthetic vitamins.

[0097] The molecule-of-interest which is attached to the microtube of the invention can be labeled. Such a label can be an intrinsic property of the molecule-of-interest (e.g., as in the case of green fluorescent protein) or can be a label which is attached to the molecule-of-interest using known methods. For example, the label can be a fluorescent labeling in which a fluorophore (*i.e.*, an entity which can be excited by light to emit fluorescence) or a radio-isotope is conjugated via a linker or a chemical bond to the molecule-of-interest. Alternatively, the molecule-of-interest can be indirectly labeled via a covalently conjugated enzyme (e.g., horse radish peroxidase) and a covalently conjugated substrate (e.g., o-phenylenediamine) which upon interaction therebetween yield a colorimetric or fluorescent color.

[0098] The molecule-of-interest can also comprise a member of an affinity pair, which is capable of reversibly or non-reversibly binding with high affinity (e.g., less than 10^{-7} M, e.g., less than 10^{-8} M, less than 10^{-9} , less than 10^{-10} M) to a specific molecule. For example, the affinity pair can be an enzyme-substrate pair, a polypeptide-polypeptide pair (e.g., a hormone and receptor, a ligand and receptor, an antibody and an antigen, two chains of a multimeric protein), a polypeptide-small molecule pair (e.g., avidin or streptavidin with biotin, enzyme-substrate), a polynucleotide and its cognate polynucleotide such as two polynucleotides forming a double strand (e.g., DNA-DNA, DNA-RNA, RNA-DNA), a polypeptide-polynucleotide pair (e.g., a complex formed of a polypeptide and a DNA or RNA e.g., aptamer), a polypeptide-metal pair (e.g., a protein chelator and a metal ion), a polypeptide and a carbohydrate (leptin-carbohydrate), and the like.

[0099] The molecule-of-interest, which is comprised within the second polymeric solution, can be attached to the coat

over the internal surface of the shell. For example, as shown in Figure 5 and described in Example 3 of the Examples section which follows, most of the β -GAL enzymatic activity was detected inside the microtube, demonstrating the attachment of the enzyme to the coat over the internal surface of the shell.

5 [0100] During the electrospinning process some molecules-of-interest which are comprised within the second polymeric solution may migrate to the outer surface of the shell (i.e., mixed with the first polymeric solution) depending on their charge state, size and geometry. For example, as shown in Figure 3 and described in Example 2 of the Examples section which follows, some of the alkaline phosphatase activity was detected in the rinsing buffer of the microtube.

10 [0101] According to some embodiments of the invention attachment of the molecule-of-interest is performed following microtube formation. For example, the microtube can be soaked with a solution containing the molecule-of-interest. The molecule-of-interest can diffuse through the shell pores and enter the inner lumen of the microtube. In addition, the microtube can be covalently attached to the molecule-of-interest (e.g., via SH groups).

[0102] Regardless of the method of production, the present invention provides a microtube which comprises an electrospun shell, an electrospun coat over an internal surface of the shell and a molecule-of-interest attached to the microtube.

15 [0103] As used herein, the phrase "electrospun shell" refers to a hollow element of a tubular shape, made of one or more polymers, produced by the process of electrospinning as detailed above.

[0104] As used herein the phrase "electrospun coat" refers to a thin layer covering the internal surface of the shell of the microtube of the invention which is made of one or more polymers by the process of electrospinning as detailed above.

20 [0105] One of ordinary skill in the art will know how to distinguish an electrospun object from objects made by means which do not comprise electrospinning by the high orientation of the macromolecules, the skin (e.g., shell) morphology, and the typical dimensions of the microtube which are unique to electrospinning.

[0106] The microtube of the invention can be an individual (e.g., single or separated) microtube or can form part of a plurality (e.g., an aligned array) of microtubes which can be either connected to each other or separated (as single, not-connected microtubes).

25 [0107] For the production of a single microtube a fork like clip is attached to the edge of the rotating disk. The disk is rotated for 1-2 seconds and individual microtubes are formed between the sides of the clip. In a similar way individual electrospun fibers were collected (see E. Zussman, M. Burman, A.L. Yarin, R. Khalfin, Y. Cohen, "Tensile Deformation of Electrospun Nylon 6,6 Nanofibers," Journal of Polymer Science Part B: Polymer Physics, 44, 1482-1489, 2006).

30 [0108] Alternatively, when using a rotating collector, a plurality of microtubes can be formed and collected on the edge of the collector as described elsewhere for electrospun fibers (A. Theron, E. Zussman, A.L. Yarin, "Electrostatic field-assisted alignment of electrospun nanofibers", Nanotechnology J., 12, 3: 384-390, 2001).

35 [0109] The plurality of microtubes can be arranged on a single layer, or alternatively, the plurality of microtubes define a plurality of layers hence form a three dimensional structure. The microtubes can have a general random orientation, or a preferred orientation, as desired. For example, when the fibers are collected on a cylindrical collector such as a drum, the microtubes can be aligned predominantly axially or predominantly circumferentially. Different layers of the electrospun microtubes can have different orientation characteristics. For example, without limiting the scope of the present invention to any specific ordering or number of layers, the microtubes of a first layer can have a first predominant orientation, the microtubes of a second layer can have a second predominant orientation, and the microtubes of third layer can have general random orientation.

40 [0110] The microtube of the invention can be available as a dry fibrous mat(s) (e.g., as spun dry microtubes) or as a wetted mat(s) (e.g., following immersing or filling the microtube with a liquid).

45 [0111] The microtube of the invention which is attached to the molecule-of-interest may be configured as or in a microfluidics device. "Lab-on-a-chip" is described in a series of review articles [see for example, Craighead, H. Future lab-on-a-chip technologies for interrogating individual molecules. Nature 442, 387-393 (2006); deMello, A. J. Control and detection of chemical reactions in microfluidic systems. Nature 442, 394-402 (2006); El-Ali, J., Sorger, P. K. & Jensen, K. F. Cells on chips. Nature 442, 403-411 (2006); Janasek, D., Franzke, J. & Manz, A. Scaling and the design of miniaturized chemical-analysis systems. Nature 442, 374-380 (2006); Psaltis, D., Quake, S. R. & Yang, C. H. Developing optofluidic technology through the fusion of microfluidics and optics. Nature 442, 381-386 (2006); Whitesides, G. M. The origins and the future of microfluidics. Nature 442, 368-373 (2006); Yager, P. et al. Microfluidic diagnostic technologies for global public health. Nature 442, 412-418 (2006)].

50 [0112] According to some embodiments of the invention, the liquid which fills in, flows in or surrounds the microtube enables the desorption (detachment) of the molecule-of-interest from the microtube (e.g., from the polymer included in the coat over the internal surface of the shell). According to of some embodiments of the invention the desorption process facilitates the interaction between the molecule-of-interest and a substrate. According to some embodiments of the invention the desorption process enables the flow and/or the release of the molecule-of-interest within and/or from the microtube.

55 [0113] According to some embodiments of the invention, the molecule-of-interest which is attached to the microtube of the invention remains active, i.e., maintains the activity, or at least a portion thereof, which it possessed prior to the attachment (e.g., of the same molecule-of-interest before electrospinning, or when not-attached to the microtube). The

term "activity" as used herein refers to any of a catalytic activity, kinetics, and/or affinity to a substrate, a ligand or an affinity member of the molecule. Such an activity can be any biological activity such as catalysis, binding (with a specific affinity), hybridization, chelation, degradation, synthesis, catabolism, hydrolysis, polymerization, transcription, and the like.

5 **[0114]** As used herein the phrase "at least a portion of the activity" refers to at least about 10 %, at least about 20-50 %, e.g., more than about 50 %, e.g., more than about 60 %, e.g., more than about 70 %, e.g., more than about 75 %, e.g., more than about 80 %, e.g., more than about 90 %, e.g., more than about 95 % of the activity which the molecule-of-interest possessed prior to the attachment to the microtube.

10 **[0115]** For example, as mentioned before and described in the Examples section which follows, the enzymes contained within the microtubes preserved the specific activity to their substrates at a kinetic which is comparable (*i.e.*, within the same order of magnitude) to that of the enzyme in the polymeric solution prior to electrospinning.

[0116] The microtube of the invention which is attached to an active molecule-of-interest can be used in various applications which require the attachment of active molecules (e.g., enzymes, DNA, RNA) to a support and optionally also the controlled release therefrom.

15 **[0117]** According to some embodiments of the invention, the microtube of the invention is attached to more than one type of molecule-of-interest. The combination of molecules can be selected according to the intended use. For example, several molecules (e.g., enzymes) which are involved in complex reactions (e.g., processing of a substrate or a mixture of substrates) can be used.

20 **[0118]** Thus, according to an aspect of the invention, there is provided a method of processing a substrate-of-interest. The method is effected by contacting the substrate-of-interest with the microtube of the invention, wherein the molecule-of-interest is capable of processing the substrate, thereby processing the substrate-of-interest.

[0119] As used herein the term "processing" refers to a catalytic activity performed by the molecule-of-interest which is attached to the microtube on its cognate substrate.

25 **[0120]** According to some embodiments of the invention, such a process can concomitantly incorporate of the substrate-of-interest in a synthesis reaction catalyzed by the molecule-of-interest.

30 **[0121]** For example, the microtube of some embodiments the invention can be used as a micro-reactor (e.g., bioreactor) for chemical transition reactions requiring high concentrations of several enzymes. As described in Example 4 of the Examples section which follows and schematically illustrated in Figure 9, the microtube of the invention can be attached to certain molecules (enzymes in this case), which together catalyze a multi-step synthesis reaction (e.g., cascade) which converts an initial substrate (e.g., compound A) to an end-product (e.g., compound E). As mentioned, the selective shell of the microtube can be designed such that it prevents the leakage (escape by diffusion) of the intermediate compounds (e.g., compounds B, C and D) therethrough and thus enables sufficiently high concentrations of such compounds as needed for the synthesis of the end product. The local concentration of the intermediate molecules formed from the initial substrate (entrapped at the time of spinning or externally added after electrospinning to the formed microtube) are about 2-10 orders of magnitude greater than the concentrations formed in an open system. Thus, the microtube of some embodiments of the invention exhibits a great kinetic advantage in multi-step reactions as compared to an open system. Microtubes are in this way similar to living cells which function on the same principle.

35 **[0122]** For example, to synthesize an indole-glycerol phosphate, an intermediate compound in tryptophan synthesis within cells, a microtube of some embodiments of the invention can be attached to the enzymes anthranilate-phosphoribosyl transferase (EC 2.4.2.18), phosphoribosylanthranilate isomerase (EC 5.3.1.24) and indole-3-glycerol-phosphate synthase (EC 4.1.1.18), and the reaction commences when anthranilate and phosphoribosyl-pyrophosphate interact with the attached enzymes. The substrates (anthranilate and phosphoribosyl-pyrophosphate) can be either added externally to the reaction medium (within which the microtube is placed) or can be attached to the microtube by mixing them within the second polymeric solution. When the substrates are supplied externally, pores of about 2-20 nm in diameter should exist in the shell to allow diffusion of anthranilate and phosphoribosyl-pyrophosphate therethrough.

45 **[0123]** According to some embodiments of the invention, such a process can be the incorporation of the substrate-of-interest in a catabolism reaction catalyzed by the molecule-of-interest.

50 **[0124]** A catabolism reaction can be the degradation (e.g., by hydrolysis) of a toxic molecule for the purpose of detoxification (e.g., detoxifying water) or decomposition of an unwanted molecule. Examples include, but are not limited to, the removal of the chlorine entity from atrazine (see Figure 10) and the degradation of cyanide resulting from silver mining.

[0125] According to an aspect of the invention, there is provided a method of depleting a molecule from a solution. The method is effected by contacting the solution with the microtube of the invention, wherein the member of the affinity pair (which is attached to the microtube) is selected capable of binding the molecule (which is to be removed), thereby depleting the molecule from the solution.

55 **[0126]** According to an embodiment of the invention, the method further comprising collecting the solution following the contacting.

[0127] As used herein the phrase "depleting" refers to removing an amount e.g., at least about 50 %, at least about

60 %, at least about 70 %, at least about 80 %, at least about 90 %, at least about 95 %, e.g., 99 %, e.g., 100 % of the molecule from the solution.

[0128] According to some embodiments of the invention, the depletion (removal) of the molecule from the solution is effected within a short time period, such as within minutes (e.g., 1-30 minutes), hours (e.g., 1-10 hours) or several days (e.g., 1-5 days).

[0129] As used herein the phrase "contacting" refers to enabling the interaction between the molecule and the member of the affinity pair, which is attached to the microtube, for a time period which is sufficient for depleting the molecule from the solution. Such a contact can take place while the solution is passing through (e.g., via capillary forces) the end(s) of the hollow structure of the microtube and/or through the shell pores. Additionally or alternatively, such a contact between the molecule and the member of the affinity pair can take place by incubating the microtube in the solution (e.g., by placing the microtube in a container including the solution).

[0130] The solution can be any water-based solution which includes inorganic or organic molecules, such as a biological sample or a sample from a non-living source such as stream or ocean waters. As used herein the phrase "biological sample" refers to any sample derived from a living organism such as plant, bacteria or mammals, and can include cells or alternatively be cell-free (i.e., include only a biological fluid). For example, a biological sample of an individual can include body fluids such as blood or components thereof (e.g., white blood cells, red blood cells, coagulation factors, leukocytes, neutrophils, serum, plasma), cerebrospinal fluid, urine, lymph fluids, and various external secretions of the respiratory, intestinal and genitourinary tracts, tears, saliva, milk, amniotic fluid and chorionic villi, a tissue biopsy, a tissue section, a malignant tissue, and the like. The sample can be derived from the individual and be further tested *in vitro* or *ex vivo*, or alternatively, can be not physically removed from the subject (e.g., for *in situ* detection and/or diagnosis).

[0131] According to some embodiments of the invention, the solution is an aqueous solution such as a drinking water, a groundwater and/or an industrial waste water. According to some embodiments of the invention, the microtube of the invention forms part of an aqueous system designed for treatment of the aqueous solution (e.g., for depleting, eliminating or removing toxic moieties therefrom).

[0132] For example, to remove a certain metal ion (e.g., copper, gold, nickel, zinc, lead, mercury, cadmium, silver, iron, manganese, palladium, and platinum) from water, the microtube of the invention can be attached to a water soluble ethylene dichloride ammonia polymer, which contains dithiocarbamate salt groups and is capable of chelating the metal ion (US Pat. No. 5,346,627). Thus, by contacting the water with the microtube the ethylene dichloride ammonia polymer binds to the metal ion and removes it from the water. Water collected after being in contact with the microtube is substantially devoid of the metal ion. Alternatively, these metal ions may be removed by attaching a protein chelator of such metal ions to the microtube.

[0133] Alternatively, to remove a ligand (e.g., a hormone, a substrate, a co-factor or a vitamin such as biotin) from a solution containing a biological sample, the microtube can be attached to a polypeptide which is member of an affinity pair such as an enzyme, a hormone or streptavidin, and following contacting the solution with the microtube, the ligand remains attached to the microtube while the solution is substantially devoid of the ligand (e.g., includes less than 0.5 %, e.g., less than 0.1 %, e.g., less than 0.01 % of the ligand).

[0134] According to some embodiments of the invention, the molecule which is to be removed from the solution comprises an antigen and the member of the affinity pair comprises the antibody capable of specifically binding the antigen.

[0135] For example, the microtube of the invention can be used to remove virus particles from a blood sample. Briefly, an anti-virus antibody (e.g., anti-HIV antibodies such as those described in Tullis, RH., et al., Therapeutic Apheresis and Dialysis, 6: 213-220) can be attached to the microtube and a blood sample containing the virus particles (e.g., HIV particles) can be in contact with the microtube such that the virus particles bind to their respective antibodies and the collected blood sample (after being in contact with the microtube) is substantially devoid of the viral particles.

[0136] The member of the affinity pair which is attached to the microtube of the invention can be also used to isolate a molecule from a solution.

[0137] According to an aspect of the invention, there is provided a method of isolating a molecule from a solution. The method is effected by: (a) contacting the solution with the microtube of the invention under conditions which allow binding of the molecule to the microtube via the member of the affinity pair which is selected capable of binding the molecule, and (b) eluting the molecule from the microtube, thereby isolating the molecule from the solution.

[0138] As used herein the term "isolating" refers to physically separating the molecule from the solution or its other components by binding the molecule to the member of the affinity pair that is attached to the microtube and eluting the bound molecule therefrom. As used herein the term "eluting" refers to dissociating the bound molecule from the microtube. Those of skills in the art are capable of adjusting the conditions required for eluting (e.g., releasing) the molecule from the microtube and/or separating the molecule from the other member of the affinity pair.

[0139] As is further described in Example 5 of the Examples section which follows, the present inventors have envisaged the use of the microtube of the invention, which is attached to a member of an affinity pair, as a biosensor, for the detection of molecules in a sample. Such a biosensor can be advantageous over known open field biosensors (e.g., sensors in which the member of the affinity pair is conjugated to a solid support not having a tubular structure, such as

a flat support) due to the increased ratio between the size of the microtube surface (which attaches the member of the affinity pair) and the volume of the sample being in contact therewith.

[0140] According to an aspect of the invention, there is provided a method of detecting a presence of a molecule in a sample. The method is effected by (a) contacting the sample with the microtube of the invention, wherein the member of the affinity pair is selected capable of binding the molecule, and; (b) detecting binding of the molecule by the member of the affinity pair, thereby detecting the presence of a molecule in the sample.

[0141] As used herein the phrase "detecting binding" refers to identifying a change in the concentration, conformation, spectrum or electrical charge of the molecule in the sample and/or the member of the affinity pair that is attached to the microtube following the binding therebetween. Identification of such binding can be performed using methods known in the art such as following the fluorescence or the color of the sample, radioactivity in the sample, the electrical conductivity of the sample and the like.

[0142] As mentioned hereinabove and described in Example 2 of the Examples section which follows, the microtube of the invention can release the molecule-of-interest attached thereto (a releasing apparatus).

[0143] The microtube of some embodiments the invention (e.g., a microtube made of biocompatible polymers) can be implanted in a subject in need thereof.

[0144] As used herein the phrase a "subject in need thereof" refers to any animal subject e.g., a mammal, e.g., a human being which suffers from a pathology (disease, disorder or condition) which can be treated by the molecule that is attached to or flows through the microtube of the invention.

[0145] The term "treating" as used herein refers to inhibiting, preventing or arresting the development of a pathology and/or causing the reduction, remission, or regression of a pathology. Those of skill in the art will understand that various methodologies and assays can be used to assess the development of a pathology, and similarly, various methodologies and assays may be used to assess the reduction, remission or regression of a pathology.

[0146] Methods of implanting grafts such as the microtube of the invention into a subject are known in the art. For example, the microtube can be implanted subcutaneously, intradermally, or into any body cavity (e.g., abdomen), as well as into the vascular system (using e.g., a hollow catheter delivery system). Alternatively, the microtube of the invention can be connected to a body conduit (e.g., a blood vessel such as a vein or an artery) such that it enables the flow of a fluid therethrough.

[0147] For example, the microtube of the invention which is capable of depleting a molecule from a solution as described above, can be connected to a blood vessel of the subject. For example, the proximal end of the microtube (or of a plurality of microtubes) can be connected to a feeding blood vessel and the distal end of the microtube(s) can be connected to a receiving blood vessel. Such a configuration can be used, for example, for hemodialysis and depletion of a specific molecule (e.g., a virus particle such as HIV, hepatitis virus such as HCV) from the blood stream of the subject.

[0148] In addition, a microtube which is attached to a drug molecule can be implanted in a subject in need thereof to thereby release a therapeutically effective amount of the drug to cells of the subject.

[0149] As used herein the phrase "therapeutically effective amount" means an amount of the molecule-of-interest (e.g., the drug, the active molecule) effective to prevent, alleviate or ameliorate symptoms of a pathology or prolong the survival of the subject being treated. Determination of a therapeutically effective amount is well within the capability of those skilled in the art.

[0150] For example, in case the molecule-of-interest comprises a polynucleotide, such a polynucleotide can be used in gene therapy applications to either increase an expression level or activity of a desired polypeptide needed for treating the pathology, or to decrease or inhibit the expression level of a polynucleotide causing the pathology (e.g., antisense technology). Alternatively, the polynucleotide can be used to immunize the subject by inducing an immune response thereagainst.

[0151] Alternatively, in case the molecule-of-interest is a polypeptide, such a polypeptide can be used in a subject in need of polypeptide therapy, such as a subject having a decreased or no activity of the polypeptide (e.g., due to a genetic disease, auto-antibodies, pathogen infection, degeneration or a decrease in tissue functioning), as well as for other therapeutic applications such as immunization with the polypeptide.

[0152] Non-limiting examples of pathologies which require polypeptide therapy and can be treated using the microtube of the invention include, metabolic disorders such as phenylketonuria (PKU), Gaucher disease, muscular dystrophy [Duchenne (DMD) and Becker (BMD) Muscular Dystrophies], Aceruloplasminemia (an iron metabolic disorder), endocrine diseases such as diabetes, autoimmune diseases such as multiple sclerosis (MS), rheumatoid arthritis (RA), and psoriasis, and various cancers (e.g., lymphoma).

[0153] Following is a non-limiting list of polypeptides which can be attached to the microtube of the invention in order to treat pathologies requiring polypeptide therapy. Phenylalanine hydroxylase [(PAH); GenBank Accession Nos. NM_000277.1 (nucleic acid sequence) and NP_000268.1 (SEQ ID NO:3; amino acid sequence)] for treating phenylketonuria (PKU), dystrophin [(DMD); GenBank Accession Nos. NM_000109.2 (nucleic acid sequence) and NP_000100.2 (SEQ ID NO:4; amino acid sequence)] for treating Duchenne (DMD) and Becker (BMD) Muscular Dystrophies, beta-glucosidase [(GBA); GenBank Accession Nos. NM_001005741.1 (nucleic acid sequence) and NP_001005741.1 (amino

acid sequence; SEQ ID NO:5)] for treating Gaucher disease, insulin [GenBank Accession Nos. NM_000207.1 (nucleic acid sequence) and NP_000198.1 (amino acid sequence; SEQ ID NO:6)] for treating diabetes, and ceruloplasmin ferroxidase [(CP); GenBank Accession Nos. NM_000096.1 (nucleic acid sequence) and NP_000087.1 (SEQ ID NO:7; amino acid sequence)] for treating aceruloplasminemia, CD20 monoclonal antibodies for treating non-Hodgkin's lymphoma and autoimmune disease (Yazawa N, et al., 2005, Proc Natl Acad Sci USA. 102:15178-83) and T-cell receptor peptides for treating of multiple sclerosis (MS), rheumatoid arthritis (RA), and psoriasis (Vandenbark AA, et al., 2001, Neurochem Res. 26:713-30).

[0154] Targeted delivery of a drug molecule to a tissue-of-interest is desired in various pathologies, especially in cases where the effect of the drug is deleterious to non-diseased tissues or when high concentrations of drug molecules are required to achieve a therapeutic effect on the diseased tissue (the tissue-of-interest). Thus, for example it is highly desired to have a targeted delivery of a chemotherapy agent or a radiation seed particle to the liver in case of hepatic cancer, or an angiogenic factor to coronary blood vessels, heart or carotid blood vessels in case of ischemia.

[0155] According to an embodiment of the invention, for targeted delivery of a drug molecule to a tissue-of-interest via the opening of the microtube (at the targeted tissue), the microtube of the invention is designed such that the electrospun shell is semipermeable (i.e., prevents passage of the drug molecule but enables the penetration of water or a physiological solution therethrough) and the coat over the internal surface of the shell is attached to the drug molecule.

[0156] Such a microtube can be implanted in a subject such that the distal end of the microtube is implanted in or in close proximity to the tissue-of-interest. As used herein the term "proximity" refers to being in a cavity defined by the tissue, for example, if the tissue in which the drug is released is a blood vessel (artery or vein) the cavity is a lumen of such a blood vessel, or if the tissue in which the medication is released is a heart chamber, then the cavity is an atrium or a ventricle. It will be appreciated that the other end of the microtube can be also implanted in proximity to the tissue-of-interest. Alternatively, the proximal end of the microtube can be either sealed using e.g., a laser beam to prevent delivery of the drug to undesired cells/tissues of the subject, or if needed, could be placed outside the body, or subcutaneously such that the microtube can be replenished with additional drug molecules using extra thin needles (e.g., which can penetrate a 5 μ m lumen of the microtube).

[0157] Once the microtube of some embodiments of the invention (e.g., a microtube with a semi permeable shell and a drug molecule attached to the coat over the internal surface of the shell) is implanted in the subject it can be filled with a physiological fluid (e.g., of the subject) which is capable of dissolving the water-soluble polymer of the coat over the internal surface of the shell to thereby release the drug molecule therefrom. The released drug molecule flows by capillary forces within the microtube until reaching the end of the open lumen, which is in proximity of the tissue-of-interest.

[0158] If needed, the microtube according to this embodiment of the invention, can be also replenished with additional drug molecules or other molecules which can increase the effect of the drug molecule released by the microtube. For example, if the drug molecule attached to the microtube is an angiogenic factor, a solution saturated with gasses (e.g., oxygen) can be administered to the microtube (e.g., after implantation in the subject) to thereby increase the anti-ischemic effect of the angiogenic factor.

[0159] Targeted delivery of a drug to a tissue-of-interest can be also effected using a microtube in which the shell enables diffusion of the drug molecule therethrough and accordingly, the drug molecule can be released through the shell pores and/or the distal opening of the microtube at the desired tissue.

[0160] The invention further envisages the use of the microtube of the invention, which include a molecule-of-interest attached thereto, for guiding cell growth *ex vivo* or *in vivo*. For example, neuronal cells can be placed near or in direct contact with the microtube which is attached to necessary growth factors and nutrients needed for neuronal growth. It will be appreciated that once an initial neuronal growth has occurred *ex vivo*, such a system (i.e., the microtube and the neuronal cells) can be implanted in a subject in need thereof (e.g., a subject with degenerated, damaged or injured neuronal cells) to thereby enable neuronal growth and guidance.

[0161] The microtube of some embodiments of the invention can be included in a kit/ article of manufacture along with a packaging material and/or instructions for use in any of the above described methods or applications.

[0162] As used herein the term "about" refers to $\pm 10\%$.

[0163] The terms "comprises", "comprising", "includes", "including", "having" and their conjugates mean "including but not limited to". This term encompasses the terms "consisting of" and "consisting essentially of".

[0164] The phrase "consisting essentially of" means that the composition or method may include additional ingredients and/or steps, but only if the additional ingredients and/or steps do not materially alter the basic and novel characteristics of the claimed composition or method.

[0165] As used herein, the singular form "a", "an" and "the" include plural references unless the context clearly dictates otherwise. For example, the term "a compound" or "at least one compound" may include a plurality of compounds, including mixtures thereof.

[0166] Throughout this application, various embodiments of this invention may be presented in a range format. It should be understood that the description in range format is merely for convenience and brevity and should not be construed as an inflexible limitation on the scope of the invention. Accordingly, the description of a range should be

considered to have specifically disclosed all the possible subranges as well as individual numerical values within that range. For example, description of a range such as from 1 to 6 should be considered to have specifically disclosed subranges such as from 1 to 3, from 1 to 4, from 1 to 5, from 2 to 4, from 2 to 6, from 3 to 6 etc., as well as individual numbers within that range, for example, 1, 2, 3, 4, 5, and 6. This applies regardless of the breadth of the range.

5 **[0167]** Whenever a numerical range is indicated herein, it is meant to include any cited numeral (fractional or integral) within the indicated range. The phrases "ranging/ranges between" a first indicate number and a second indicate number and "ranging/ranges from" a first indicate number "to" a second indicate number are used herein interchangeably and are meant to include the first and second indicated numbers and all the fractional and integral numerals therebetween.

10 **[0168]** As used herein the term "method" refers to manners, means, techniques and procedures for accomplishing a given task including, but not limited to, those manners, means, techniques and procedures either known to, or readily developed from known manners, means, techniques and procedures by practitioners of the chemical, pharmacological, biological, biochemical and medical arts.

15 **[0169]** An electrospinning apparatus can include a controller programmed with parameters as described herein or measuring output and automatically modifying. Controller can be hardware, software, firmware, with CPU, volatile memory, optional non-volatile memory.

20 **[0170]** It is appreciated that certain features of the invention, which are, for clarity, described in the context of separate embodiments, may also be provided in combination in a single embodiment. Conversely, various features of the invention, which are, for brevity, described in the context of a single embodiment, may also be provided separately or in any suitable subcombination or as suitable in any other described embodiment of the invention. Certain features described in the context of various embodiments are not to be considered essential features of those embodiments, unless the embodiment is inoperative without those elements.

[0171] Various embodiments and aspects of the present invention as delineated hereinabove and as claimed in the claims section below find experimental support in the following examples.

25 **EXAMPLES**

[0172] Reference is now made to the following examples, which together with the above descriptions, illustrate some embodiments of the invention in a non limiting fashion.

30 **[0173]** Generally, the nomenclature used herein and the laboratory procedures utilized in the present invention include molecular, biochemical, microbiological and recombinant DNA techniques. Such techniques are thoroughly explained in the literature. See, for example, "Molecular Cloning: A laboratory Manual" Sambrook et al., (1989); "Current Protocols in Molecular Biology" Volumes I-III Ausubel, R. M., ed. (1994); Ausubel et al., "Current Protocols in Molecular Biology", John Wiley and Sons, Baltimore, Maryland (1989); Perbal, "A Practical Guide to Molecular Cloning", John Wiley & Sons, New York (1988); Watson et al., "Recombinant DNA", Scientific American Books, New York; Birren et al. (eds) "Genome Analysis: A Laboratory Manual Series", Vols. 1-4, Cold Spring Harbor Laboratory Press, New York (1998); methodologies as set forth in U.S. Pat. Nos. 4,666,828; 4,683,202; 4,801,531; 5,192,659 and 5,212,057; "Cell Biology: A Laboratory Handbook", Volumes I-III Cellis, J. E., ed. (1994); "Current Protocols in Immunology" Volumes I-III Coligan J. E., ed. (1994); Stites et al. (eds), "Basic and Clinical Immunology" (8th Edition), Appleton & Lange, Norwalk, CT (1994); Mishell and Shiigi (eds), "Selected Methods in Cellular Immunology", W. H. Freeman and Co., New York (1980); available immunoassays are extensively described in the patent and scientific literature, see, for example, U.S. Pat. Nos. 3,791,932; 3,839,153; 3,850,752; 3,850,578; 3,853,987; 3,867,517; 3,879,262; 3,901,654; 3,935,074; 3,984,533; 3,996,345; 4,034,074; 4,098,876; 4,879,219; 5,011,771 and 5,281,521, "Oligonucleotide Synthesis" Gait, M. J., ed. (1984); "Nucleic Acid Hybridization" Hames, B. D., and Higgins S. J., eds. (1985); "Transcription and Translation" Hames, B. D., and Higgins S. J., Eds. (1984); "Animal Cell Culture" Freshney, R. I., ed. (1986); "Immobilized Cells and Enzymes" IRL Press, (1986); "A Practical Guide to Molecular Cloning" Perbal, B., (1984) and "Methods in Enzymology" Vol. 1-317, Academic Press; "PCR Protocols: A Guide To Methods And Applications", Academic Press, San Diego, CA (1990); Marshak et al" "Strategies for Protein Purification and Characterization - A Laboratory Course Manual" CSHL Press (1996). Other general references are provided throughout this document. The procedures therein are believed to be well known in the art and are provided for the convenience of the reader.

50 **GENERAL MATERIALS AND EXPERIMENTAL METHODS**

55 **[0174] Enzymes and solutions** - The compositions of the shell and core solutions are given in Table 3, hereinbelow. All polymers and solvents were purchased from Sigma-Aldrich and were used as is. Alkaline phosphatase (AP) and beta-galactosidase (β -GAL) from *E. coli* were also purchased from Sigma-Aldrich. AP cleaves monophosphate esters and has a molecular weight of about 80,000 Da. β -GAL is a tetrameric enzyme of 465,396 Da consisting of four identical subunits each (Zabin I., et al., 1980) and catalyzes the hydrolysis of the terminal galactosidyl group of β -galactosides. Both enzymes were initially dissolved in water and then mixed with the core solution.

Table 3

<i>Two types of core-shell microtubes composition of the solutions</i>		
<i>Type</i>	<i>Shell solution</i>	<i>Core solution</i>
1	10 % PCL 80 K; in CHCl ₃ :DMF (90:10 by weight)	4 % (w/w) PEO 600 K + 0.0733 mg/ml AP or 2.38 units/ml β-GAL; in ethanol:H ₂ O (26:74 by weight)
2	10% PCL 80 K +1 % PEG 6 K; in CHCl ₃ :DMF (90:10 by weight)	4 % (w/w) PEO 600 K + 0.0733 mg/ml AP or 2.38 units/ml β-GAL; in ethanol:H ₂ O (26:74 by weight)

Table 3. Microtubes were formed by co-electrospinning of the shell solution (a first polymeric solution for forming the shell) and a core solution (a second polymeric solution for forming the coat over the internal surface of the shell).

[0175] Electrospinning - Hollow microtubes (core-shell hollow fibers) were fabricated by a co-electrospinning process using the set up described by Sun et al. 2003 and Zussman et al. 2006. All experiments were conducted at room temperature (about 22 °C) and a relative humidity of about 35 %. The spinning parameters were as follow: the electrostatic field used was approximately 0.44 kV/cm and the distance between the spinneret and collector plate was 16 cm. The flow rates of both the core and shell solutions were controlled by two syringe pumps and were 3.5 ml/hour for the shell solution and 1 ml/hour for the core solution. The fibers were collected as a strip on the edge of a vertical rotating wheel (Theron A., et al., 2001) having a velocity of 1.2 m/second. For fluorescence microscopy, a few fibers were collected directly onto a microscope slide

[0176] Imaging - Images of the fibers were obtained using a Leo Gemini high resolution scanning electron microscope (HRSEM) at an acceleration voltage of 3 kV and a sample to detector distance of 3-5 mm. The specimens were coated with a thin gold film to increase their conductivity. Fluorescence microscope Leica DM IRE2 at excitation and emission wave lengths of 359 and 361 nm, respectively, was used for the imaging of fibers filled with fluorescent product.

[0177] Measurement of the Enzyme Activity - To measure enzyme activity, pieces of mat were weighed and dipped in assay solution according to Table 4, hereinbelow. At each time of sampling, the solution was mixed with a vortex mixer, and 1 ml of the assay mixture was transferred to spectrophotometer cuvette. The absorbance of the solution was measured in a Perkins-Elmer spectrophotometer at a wavelength of 410 nm. For both enzymatic reactions, the substrates are colorless but the products, para-nitrophenol for AP and ortho-nitrophenol for β-GAL, are yellow with an absorption maximum at 410 nm. After the absorbance was measured, the liquid was returned to the assay vessel. Units, activity and relative activity are defined as follow:

$$(1) \quad \text{Unit} = \frac{\Delta A}{\Delta t} \cdot 1000$$

$$(2) \quad \text{Activity of the mat} = \text{unit} \cdot C$$

where

$$C = \frac{\text{mass of total mat}}{\text{mass of piece}}$$

$$(3) \quad \text{Relative Activity (\%)} = \frac{\text{Activity of the mat}}{\text{Activity of the core solution}} \cdot 100$$

[0178] Where: ΔA is the difference is the absorbance at difference times, Δt , difference between t_1 and t_2 (two time points) taken in the linear region of the reaction curve, and C is a normalization factor which takes into account the different weight of each piece.

[0179] For the fluorescence microscope imaging a drop of the assay solution was put directly on the microscope slide

on which a few fibers had been deposited. The fluorescent substrates were methylumbelliferyl-phosphate for alkaline phosphatase (AP) and methylumbelliferyl-galactoside for beta-galactosidase (β -GAL). These were used at the same concentrations as their nitro-phenyl analogs.

Table 4

<i>Composition of the assays</i>				
<i>Enzyme</i>	<i>Substrate</i>	<i>Buffer</i>	<i>H₂O</i>	<i>Products</i>
AP	0.7 mg/ml p-nitrophenyl-phosphate (MW = 217 Da) 1 ml	TRIS-HCl buffer 1.5 ml	0.5 ml	p-nitrophenol + PO ₄
	4-methylumbelliferyl-phosphate: fluorescence microscopy			4-methylumbelliferono + PO ₄
β -GAL	4 mg/ml o-nitrophenyl- β -D-galactoside 0.2 ml (MW = 301 Da)	Z-buffer 0.7 ml	0.3 ml	o-nitrophenol + galactose
	4-methylumbelliferyl- β -D-galactoside: fluorescence microscopy			4-methylumbelliferone + galactose

EXAMPLE I**ATTACHMENT OF ENZYMES TO ELECTROSPUN MICROTUBES****Experimental Results**

[0180] Formation of micro-tubes - Two types of electrospun hollow fibers have been fabricated with the polymers listed in Table 3, hereinabove. The resultant fibers are hollow structures, namely micro-tubes, as previously described by the present inventors (Dror, Y et al., 2007 and PCTABM07/054001). The hollow nature of these structures and the different morphologies of the tube walls are demonstrated in the high resolution scanning electron microscope (HRSEM) micrographs presented in Figures 1a-d. Type 1 fibers are made with only PCL in the shell and exhibit a rough surface due to the rapid evaporation of the solvent (Figures 1a and c). However, this roughness doesn't affect the intact nature of the walls. As PEG is added to the shell solution (Type 2), the walls become increasingly porous (Figures 1b and d) and pores can be seen even in the interior surface of the tubes (Figure 1b). PEG and PCL are partially miscible due to favorable, but weak, intermolecular polar-interactions (Coleman MM, et al., 1991). During fiber solidification along with the evaporation of the solvents, the concentration of the components increases and phase separation takes place. However, since the PEG has a surfactant-like character it deposits an adherent film around the PCL domains resulting in the formation of pores rather than forming solid domains of PEG.

[0181] After electrospinning the tubes form a fibrous non-woven, aligned or non-aligned mat. When the mat material is placed in an aqueous environment, the coat over the internal surface of the shell dissolves and the enzymes are released (through desorption) and become active on their substrate(s). For a further description of the desorption process see Figure 8 and Example 8 hereinbelow. This arrangement of material allows for flow-through technologies without subjecting the enzyme to the external environment and without the need for chemical attachment and can prevent loss of the entrapped enzyme.

[0182] Enzymes attached to fibers maintain normal biological activity - The kinetics of the enzymatic reaction for alkaline phosphatase was measured as described in the experimental section and is presented in Figures 2a-b. The enzymatic reaction with the fibers was compared to the free enzyme in the core solution (before electrospinning) and normalized with respect to the weight of the analyzed pieces. The results strongly indicate that the enzyme attached in the fiber (e.g., encapsulated) maintains its biological activity after electrospinning and exhibits a reaction curve similar to the free enzyme. The curves are characteristic of enzymatic reactions when there is large excess of substrate. The colored product, p-nitrophenol, diffuses out of the fibers into the surrounding medium as shown in Figure 2c (Type 1). The reaction rates of the enzyme attached (e.g., contained within) the microtubes are slightly reduced in comparison to the free enzyme. Without being bound by any theory, it is possible that the reaction rates are reduced because of the following reasons: (1) the substrate has to diffuse into the fibers in order to reach the active site of the enzyme; and/or (2) the enzyme has to diffuse outside; (3) the product has to diffuse outside in order to be detected; (4) some enzyme activity was lost during the spinning process itself. The attainment of maximum reaction velocity occurs more rapidly with Type 2 fibers, undoubtedly due to their highly porous character. Upon closer examination of the initial kinetics, it

can be seen that Type 1 fibers, which do not contain PEG in the shell, exhibit a linear reaction rate that is much reduced (inset- Figure 2b, marked by dark arrows) than Type 2 fibers (which include PEG in the shell polymer, and consequently, pores in the microtube shell). Without being bound by any theory, the initial low rate seems to result from the time required for the penetration of the substrate into the fibers since these fibers have a less porous morphology and are more hydrophobic. In the porous fibers (Type 2) the penetration of the substrate is barely hampered since the presence of PEG facilitates the wetting of the outer surface of the fibers and thereby allows the access of the aqueous substrate.

[0183] Altogether, these results demonstrate that enzymes attached to (e.g., encapsulated within) electrospun microtubes maintain their enzymatic activity.

[0184] Thus, the present technology overcomes both the problem of fiber dissolution and subsequent leaching of the enzyme and the exposure of the enzyme to harmful solvents.

EXAMPLE 2

ELECTROSPUNMICROTUBES CANRELEASE ENZYMESATTACHED THERETO

Experimental Results

[0185] **Enzyme can be leached out of the electrospun microtubes** - In order to determine whether the substrate diffuses into the fibers or the enzyme diffuses out of the fibers, 3 specimens containing alkaline phosphatase (AP) were cut out from the non-woven mat and placed in buffer. The buffer from the first sample was taken immediately and assayed (initial rinse). For the second and third samples the buffer was taken and assayed after 24 hours and 72 hours, respectively. The first sample was tested in order to evaluate if any removable enzyme resides on the outer surface of the fibers after the spinning. The relative activity of the escaped enzyme in the buffers for the two types of fibers is presented in Figure 3. The results clearly indicate that a significant fraction of the enzyme has leached out of the fibers within the first 24 hours. Hence it can be concluded that the reaction monitored for the mat (the electrospun microtubes) is a result of both in-fiber and out-fiber reactions. Interestingly however, for Type 1 fibers, which do not contain PEG in the shell, 82 % of enzyme has diffused outside the fibers within 24 hours (compared to the mat). For Type 2 fibers, which are more hydrophilic due to PEG, the leaching of the enzyme is less although by no means negligible. The results also point out, as was already mentioned, that Type 2 fibers are the most active system and attains 55 % of the activity of the free enzyme.

[0186] **Alkaline phosphatase can migrate to the outer surface of the microtubes during electrospinning** - Moreover, it is clear that some enzyme is located on the outer surface of the fibers (i.e., attached to the microtube shell) and can immediately enter the surrounding buffer upon rinsing. The migration of the enzyme to the outer surface of the fibers during the spinning is more pronounced in Type 2 and is probably due to PEG which might serve as hydrophilic conduit for the enzyme. It has been already found (Reznik SN, et al., 2006) that in the core-shell process all charges immediately accumulate at the outer surface of the shell in the drop. Ions are preferentially subjected to this migration as the electric field is applied. In the present case, the protein, which is a charged molecule, can also migrate to the outer surface during electrospinning. This may explain the relatively large quantity of enzyme that is released by rinsing.

[0187] Altogether, these results demonstrate that type 2 fibers attain more enzymatic activity as compared to type 1 fibers. In addition, the enzyme within the type 2 fibers (which include PEG in the shell) is present in both the outer surface and the inner surface of the microtubes. Thus, these results demonstrate that even though the enzyme is mixed with the core solution, it is capable of migrating into the outer surface of the shell during the electrospinning process.

EXAMPLE 3

ELECTROSPUN MICROTUBES CAN SERVE AS MICROREACTORS

Experimental Results

[0188] **β -galactosidase remains within the hollow fiber micro-reactor** - The kinetics of the β -GAL reaction were determined as described hereinabove for AP and the results are presented in Figures 4a-b. Briefly, pieces of mat (electrospun microtubes) were immersed in buffer for a quick rinse, 24 or 72 hours to determine if there is any leaching of the enzyme (Figure 5, shown are results of Type 2 as an example). Two striking differences between the AP and β -GAL series were observed (Figure 6): (i) the β -GAL reaction rate of the Type 1 mat is much slower relative to that found for AP, and the activity of AP in the type 1 mat is slower relative to that found for the activity of the free enzyme in the core solution (prior to electrospinning). In type 2, conversely, the activity of the β -GAL is higher than that of AP and the reaction velocity of the β -GAL enzyme is comparable to the free enzyme. This intense response of Type 2 is attributed to the high porosity of these fibers and their hydrophilic nature; (ii) the results shown in Figure 5 for Type 2 fibers demonstrate that the β -GAL enzyme doesn't diffuse out of the fibers even after 72 hours even though Type 2 might be

thought to be the more likely to allow the enzyme to escape. That is, the reaction takes place only within the fibers. Thus, for β -GAL, the hollow fibers act as a micro-reactor; the substrate which enters the "reactor" through the entire porous shell is cleaved by the encapsulated enzyme and the reaction product then diffuses out into the surrounding medium. Thus, without being bound by any theory it seems that the reduction in the reaction rate for Type 1 is related solely to the slow diffusion of the substrate into the fibers. The size of the enzyme seems to affect both the amount of enzyme that can migrate during the spinning to the outer surface of the fibers and its subsequent escape into the surrounding medium. In the case of β -GAL only a small amount of enzyme was detected in the rinsing buffer for Type 2 while for Type 1 no enzyme was detected at all (data not shown). As was argued before, in the fibers which do not contain PEG in the shell (Type 1) an additional moderate slope at the very beginning of the reaction can be observed (Figure 4b-inset, marked by dark arrow) due to the relatively high hydrophobicity of the surface which hinders the access of the aqueous dissolved substrate.

[0189] Altogether, these results demonstrate that the Type 1 system results in lowered enzymatic activity, especially for large proteins such as β -GAL, which cannot diffuse through the shell pores. The fact that Type 1 fibers are hydrophobic and non-porous and thus inhibit the entrance of these substrates seems to make Type 1 fibers less efficacious for their use as flow-through reactors. This is in contrast to the remarkably efficient system obtained with Type 2 fibers.

[0190] *The enzymatic reaction occurs within type 1 microtubes (hollow fibers)* - Visual evidence that the enzymatic reaction occurs within the type 1 fibers was obtained by using a substrate in which one of the products is fluorescent. For both AP and β -GAL enzymes the substrates used liberate 4-methylumbelliferone after hydrolysis which allows imaging by fluorescence microscopy. As is clearly seen in Figures 7a-b, the interior of the fibers is fluorescent while the surrounding medium is dark. Thus, these results clearly show that both enzymatic reactions (of AP and β -GAL), in fact, take place within the fibers. It is important to emphasize that, in contrast to the mat immersion experiments, this method is very sensitive and enables the detection of very small amounts of product which accumulates within a relatively short time. Indeed, these images were acquired within 1-2 minutes after the substrate was applied, a time scale which is larger than the characteristic time [about 10 seconds, as was calculated by the present inventors (Dror Y., et al., 2007)] of the diffusion through the micro-tubes wall. Hence, these results are not in contradiction to those of the mat immersion experiments in which the kinetics were followed over a much longer period during which both the product and the enzyme (in the AP case) can diffuse outside the fibers. In Figure 7b short slugs (sections) of fluorescent liquid are observed. This phenomenon has been previously found in such fibers (Dror Y., et al., 2007).

[0191] The results shown in Examples 1-3 demonstrate the direct incorporation of enzymes into micro-tubes fabricated by co-electrospinning by introduction of the enzymes into the aqueous core solution of the microtube (e.g., PEO). The shell solution in this case was made of PCL dissolved in mixture of chloroform and DMF. The separation between the outer organic and inner aqueous phases was found to preserve enzyme activity during and after spinning when the electrospun fibers (mats) were subsequently placed in an aqueous environment.

[0192] Two types of micro-tubes were fabricated which differ in their shell morphology. Type 2 shells were produced by adding PEG to the shell solution. By using a mixture of PEG and PCL in the shell, pores were formed during the solidification process and this, in turn, directly affected the transfer of molecules into and out of the fibers. As a consequence, the more porous fibers (Type 2) exhibited higher rates of enzymatic reaction. In addition two enzymes differing in their molecular weight were incorporated: AP and β -GAL. The difference in the molecular weight between the enzymes was well reflected in the kinetics of the enzymatic reactions for both types of micro-tubes. While AP could diffuse outside the fibers, β -GAL remained in the fibers without any leaching of the enzyme and the progress of the reaction depended only on the arrival of the substrate from the surroundings. Thus, the AP fibers act as an enzyme release device in which the release rate can be tailored by modifying the morphology of the shell and, on the other hand, the β -GAL fibers act as an enzymatic micro-reactor with an efficient provision of the substrate through the entire surface area and efficient discharge of the product. Thus, by manipulating the morphology of the shell, the substrate supply and product release rate can be controlled. This method of encapsulation can be used when a separation between the enzyme and an external aqueous environment is desired (e.g. with living tissue to avoid immunological reactions). The remarkable retention of the enzyme activity for β -GAL Type 2 fibers clearly demonstrates that this approach preserves the activity of the enzyme.

[0193] Another advantage of the core-shell fiber method is the small volume within the micro-tubes which enables the quick buildup of the product. This is important for enzymes working in sequence where the local concentration of the product of the first reaction serves as the substrate for a subsequent reaction. In this regard, these nanotubes are somewhat analogous to living cells except that any manner of enzymes may be added to the fibers without regard to their biological origin. Another advantage of this system is that unlike living cells, there is no discrimination as to which type of small molecules may enter these tubes. For example, phosphorylated molecules (like p-nitrophenyl phosphate) which do not enter *Escherichia coli* cells can enter the microtubes described herein.

EXAMPLE 4**USE OF THE ELECTROSPUN MICROTUBES AS MICROREACTORS FOR CHEMICAL TRANSITIONS**

5 **[0194] *The microtubes of the invention as reactions for multi-step enzymatic processes*** - In order to synthesize or catabolize molecules which require multi-step enzymatic processes the present inventors have devised electrospun microtubes which include the enzymes participating in the multi-step enzymatic process, attached thereto, as follows.

10 **[0195]** For a biochemical pathway which involves the conversion of A to E via compounds B, C and D, the second polymeric solution for forming the coat over the internal surface of the shell (also referred to as a core solution) is mixed with the following enzymes: the enzyme that converts the starting substrate A to intermediate compound B, the enzyme that converts B to C, the enzyme that converts C to D, and the enzyme that converts D to the end product E (see for example, Figure 9). It should be noted that due to the proximity of the enzymes to each other in the microtube (which can be a closed micro-reactor), the local concentrations of each of the intermediate molecules, *i.e.*, compounds B, C, and D is relatively high, which enables the kinetics of the reactions to occur, similarly to their concentrations in cells or cell compartments (e.g., mitochondria). The shell solution is made from hydrophobic polymers (water insoluble polymers), with or without the addition of PEG.

15 **[0196]** Thus, the microtube of the invention enables higher local concentrations of intermediate compounds which can not be reached from the same starting material (substrate A) if an open system (such as any solid substrate to which an enzyme is immobilized) is used.

20 **[0197]** The creation of micro- and nano-fibers containing enzymes simulates the cellular structure because two or more different enzymes involved in a particular synthesis or degradation can be put into proximity of one another. The interior of the tube is quite parallel to that of cells except that the borders of the tube are made from a water insoluble substance whereas living cells are encompassed by lipid membranes. In addition the microtubes are much longer than cells but quite similar in other dimensions to a bacterial cell. In the electrospun fibers, any small molecule can pass through the water insoluble barrier (pores can be made) regardless of its chemistry with the only provision that the small molecule be water soluble.

25 **[0198]** Thus, the present technology allows the entrapment of high concentrations of an enzyme or several enzymes within a confined space. Single or multi-step reactions can then take place where the product of one reaction is the substrate of a second and the second enzyme is spatially nearby. While such multi-step reactions can occur in an open system, the time necessary to reach the end product is orders of magnitude greater than within the microtube of the invention.

30 **[0199] *The microtubes of the invention can include enzymes from different species*** - Another very important advantage of these electrospun fibers is that there is no limitation of which enzymes can be embedded. In nature, cells contain enzymes useful for their growth and reproduction. Organisms have not been designed or selected for industrial processes desired by humans. The microtubes of the invention allow any desired combination of enzymes to be brought together. This might mean that enzymes from totally different organisms (e.g. flies and humans) could be placed together for some use while in nature no organism exists with this combination.

35 **[0200] *The microtubes of the invention as micro-reactors for the production of molecules which are intermediate compounds of a natural process*** - The enzymes encapsulated might be those carrying out part of pathway making the end product a substance that is usually an intermediate molecule in living organisms. This allows one to synthesize molecules that cannot be obtained in any amount from living material because the concentration of intermediates in cells is usually very low (in the order of 10 μ M or less). For example, to synthesize indole-glycerol phosphate which is an intermediate in tryptophan synthesis within the cells of lower organisms, the enzymes that participate in the conversion of anthranilate (an inexpensive compound) to indole-glycerol phosphate should be included in the microtube, while the enzymes that continue the synthesis of tryptophan from indole-glycerol phosphate are excluded from the microtube. In summary, many combinations of enzymes from different organisms may be put together without any genetic engineering and partial sets of enzymes can also be used. The number of possible useful combinations is therefore very large.

40 **[0201]** Thus, the microtubes of the invention can be used as enzymatic micro-reactors where the inner space enables a confined but free reaction space. The substrate diffuses through the shell to the inner space where the enzymatic reaction takes place and the product can then diffuse out.

EXAMPLE 5**THE ELECTROSPUN MICROTUBES AS BIOSENSORS**

55 **[0202]** Since the electrospun microtubes of the invention are insoluble in aqueous solutions, they can provide an excellent tool for the construction of biosensors.

[0203] Since any enzyme or combination of enzymes can be encapsulated in the electrospun microtubes, a variety of biosensors can be devised. For example, enzymes that are sensitive to heavy metals exhibit loss of activity in the presence of heavy metals. Another example, firefly luciferase, for example can be electrospun with its luciferin cofactor and any reaction affecting ATP production can be used in conjunction with light output the signal.

EXAMPLE 6

THE ELECTROSPUN MICROTUBES FOR FLOW-THROUGH APPLICATIONS

[0204] **Water purification or detoxification** - The electrospun microtubes of the invention, which are made of a water-insoluble outer shell, enable the flow of liquids. It will be appreciated that enzymes embedded in such microtubes can be used to purify the liquid flowing past the microtubes as molecules diffuse in and out of them.

[0205] Thus the present inventors have devised water purification or detoxification apparatuses, as follows. The second polymeric solution which forms the coat over the internal surface of the shell (also referred to as a core solution) [which is made of water-soluble polymer(s)] includes enzymes which remove a toxic moiety from water, such as the gene product of the *atzA* gene from *Pseudomonas* ADP that removes the chlorine from atrazine, a toxic substance. The shell solution [which is made of water-insoluble polymer(s)] is designed so as to enable water flow within the microtube. The effluent would thereby be rendered free of atrazine and safe for animal and human consumption.

[0206] **Dialysis** - The microtubes of the invention can be used in various applications which remove certain compounds, such as dialysis procedures on humans. Thus, the electrospun microtubes can be made using a shell polymer which prevents the diffusion of enzymes therethrough, yet enables passage of water and substances that need to be purified. It will be appreciated that such microtubes can be also implanted into a subject in need thereof (e.g., a subject in need of dialysis), and due to the structure of a closed conduit, which prevents passage of embedded enzymes through the shell, there is no immune response to the implanted conduit.

EXAMPLE 7

THE ELECTROSPUN MICROTUBES FOR ENZYME THERAPY

[0207] Since the electrospun microtubes of the invention are insoluble in aqueous solutions, they should provide excellent tool for the construction of material for enzyme therapy. Some individuals lack certain enzymes, usually as a result of their being homozygous for recessive alleles that lead to synthesis of an inactive enzyme. Gene therapy attempts to introduce the missing active gene which thereby leads to the production of an active enzyme. However, this technique is still quite inefficient. A different way of treating such patients is enzyme therapy, in which the missing enzyme is exogenously supplied to the subject. The main drawbacks of the second method is that injection of enzymes often leads to the formation of antibodies against them and the half-life of the enzymes within the body may be quite short.

[0208] Thus, the present inventors have devised an apparatus for enzyme therapy, as follows. Briefly, the electrospun microtubes which include a water-insoluble shell can include enzymes which are needed for enzyme therapy, and be further implanted in a subject in need thereof.

[0209] **Enzyme therapy for PKU** - Phenylketonuria (PKU) occurs in slightly less than 1 per 10000 individuals and is an autosomal recessive genetic disease caused by homozygosity of alleles encoding defective enzymes. Phenylalanine and tyrosine are amino acids that are found in most proteins. In humans, the source of these two amino acids is dietary protein. In normal individuals, excess phenylalanine is converted to tyrosine. Excess tyrosine, in turn, is broken down to fumarate and acetoacetate. Both tyrosine and phenylalanine are essential for human protein synthesis. In addition, tyrosine is the precursor of melanin (skin and eye pigment) and for certain hormone like substances such as thyroxine. Phenylketonuria is caused by the lack of the enzyme (phenylalanine 4-monooxygenase EC 1.14.16.1) that converts phenylalanine to tyrosine. The result of this defect is the accumulation of phenylalanine in the blood along with a number of compounds that are derived from it (e.g. phenylpyruvic acid and phenyllactic acid). The result is brain damage (and an IQ of 30-70) as some of these compounds are toxic. The current method of preventing deterioration of the disease is to limit the intake of phenylalanine. The present inventors have envisaged that PKU can be treated by implanting electrospun microtubes containing the missing enzyme, phenylalanine hydroxylase (PAH; GenBank Accession No. NP_00026), in a subject diagnosed with PKU, and thereby enabling the breakdown of excess phenylalanine in the subject. It will be appreciated that in this case, the microtube can be designed so as to enable release of enzyme from the inner surface through the outer shell (e.g., using PEG in the outer shell) or alternatively can be designed such that the enzyme is entrapped (or remains) within the microtubes and effects its activity there (e.g., by diffusion of the substrate or end-product through the shell pores, or microtube opening(s)). As phenylalanine hydroxylase can be phosphorylated (with a molecular weight of consists of 50,000 Da) or dephosphorylated (with a molecular weight of 49,000 Da), the size of the pores in the shell should enable passage (by diffusion) of each of these forms (e.g., about 5 nm in diameter).

Microtubes can be made with smaller pores that will prevent the loss of the enzyme which will remain within the microtube.

EXAMPLE 8

5 THE DESORPTION PROCESS

[0210] Figure 8 schematically depicts the desorption of a molecule-of-interest to the microtube of the invention. After the electrospinning process, the molecule-of-interest (e.g., a protein, an enzyme) is adsorbed to the inner side of the microtubes. As mentioned, the porosity of the microtubes can be controlled (e.g., adding PEG to the shell polymer), therefore the shell consists of nanopores (see #3 in Figure 8) with an opening to the outer surface of the microtube, which herein the pores are considered to have a cylindrical shape. When immersing the microtubes in a solution (e.g., a tissue culture medium, a physiological solution or any buffer) most nanopores opening are accessible to the solution.

[0211] Once the microtubes are immersed in the solution the nanopores are filled by the solution through capillary rise (see arrow # 1 in Figure 8). It will be appreciated that the time of the capillary rise depends on the solution rheological properties (viscosity and surface tension), the wetting angle and the geometry of the nanopore (length and radius). The solution penetrates to the microtube and start wetting and filling its entire inner volume. Desorption of the molecule-of-interest from the microtube wall depends mainly on the rate of the release of the molecule-of-interest from the polymer of the second polymeric solution. Finally, the molecule-of-interest (e.g., protein/enzymes) diffuses (see arrow # 2 in Figure 8) into the solution and released to the surroundings of the microtubes (assuming that the major release is through the microtubes envelope.

[0212] Note that the geometry (radius and length) of the nanopore is controllable, by adjusting the shell thickness, or by blending, more PEG to the shell polymer. Therefore, the release from or confinement in the microtube of the invention is controllable, e.g., in certain cases the molecule-of-interest is released from the microtube, whereas in other cases, the molecule-of-interest remains in the inner volume of the microtube. As shown in Figure 2a, a molecule-of-interest is released from the microtube of the invention in a controlled manner, which can be extended beyond 2500, minutes, e.g., for several days and months.

[0213] Although the invention has been described in conjunction with specific embodiments thereof, it is evident that many alternatives, modifications and variations will be apparent to those skilled in the art. Accordingly, it is intended to embrace all such alternatives, modifications and variations that fall within the scope of the appended claims.

[0214] In addition, citation or identification of any reference in this application shall not be construed as an admission that such reference is available as prior art to the present invention. To the extent that section headings are used, they should not be construed as necessarily limiting.

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(Additional References are cited in Text)

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SEQUENCE LISTING

[0216]

- 15 <110> Technion Research & Development Foundation Ltd.
Zussman, Eyal
Dror, Yael
Kuhn, Jonathan Charles
- 20 <120> METHODS OF ATTACHING A MOLECULE-OF-INTEREST TO A MIRCROTUBE
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Arg Lys Asn Pro Lys Gly Phe Phe Leu Leu Val Glu Gly Gly Arg Ile
 325 330 335

25 Asp His Gly His His Glu Gly Lys Ala Lys Gln Ala Leu His Glu Ala
 340 345 350

Val Glu Met Asp Arg Ala Ile Gly Gln Ala Gly Ser Leu Thr Ser Ser
 355 360 365

30 Glu Asp Thr Leu Thr Val Val Thr Ala Asp His Ser His Val Phe Thr
 370 375 380

35 Phe Gly Gly Tyr Thr Pro Arg Gly Asn Ser Ile Phe Gly Leu Ala Pro
 385 390 395 400

Met Leu Ser Asp Thr Asp Lys Lys Pro Phe Thr Ala Ile Leu Tyr Gly
 405 410 415

40 Asn Gly Pro Gly Tyr Lys Val Val Gly Gly Glu Arg Glu Asn Val Ser
 420 425 430

Met Val Asp Tyr Ala His Asn Asn Tyr Gln Ala Gln Ser Ala Val Pro
 435 440 445

45 Leu Arg His Glu Thr His Gly Gly Glu Asp Val Ala Val Phe Ser Lys
 450 455 460

50 Gly Pro Met Ala His Leu Leu His Gly Val His Glu Gln Asn Tyr Val
 465 470 475 480

Pro His Val Met Ala Tyr Ala Ala Cys Ile Gly Ala Asn Leu Gly His
 485 490 495

55

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Cys Ala Pro Ala Ser Ser Ala Gly Ser Leu Ala Ala Gly Pro Leu Leu
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5 Leu Ala Leu Ala Leu Tyr Pro Leu Ser Val Leu Phe
 515 520

<210> 2

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10 <212> PRT

<213> Homo sapiens

<400> 2

15 Met Thr Met Ile Thr Asp Ser Leu Ala Val Val Leu Gln Arg Arg Asp
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Trp Glu Asn Pro Gly Val Thr Gln Leu Asn Arg Leu Ala Ala His Pro
 20 25 30

20 Pro Phe Ala Ser Trp Arg Asn Ser Glu Glu Ala Arg Thr Asp Arg Pro
 35 40 45

25 Ser Gln Gln Leu Arg Ser Leu Asn Gly Glu Trp Arg Phe Ala Trp Phe
 50 55 60

Pro Ala Pro Glu Ala Val Pro Glu Ser Trp Leu Glu Cys Asp Leu Pro
 65 70 75 80

30 Glu Ala Asp Thr Val Val Val Pro Ser Asn Trp Gln Met His Gly Tyr
 85 90 95

Asp Ala Pro Ile Tyr Thr Asn Val Thr Tyr Pro Ile Thr Val Asn Pro
 100 105 110

35 Pro Phe Val Pro Thr Glu Asn Pro Thr Gly Cys Tyr Ser Leu Thr Phe
 115 120 125

Asn Val Asp Glu Ser Trp Leu Gln Glu Gly Gln Thr Arg Ile Ile Phe
 130 135 140

40 Asp Gly Val Asn Ser Ala Phe His Leu Trp Cys Asn Gly Arg Trp Val
 145 150 155 160

45 Gly Tyr Gly Gln Asp Ser Arg Leu Pro Ser Glu Phe Asp Leu Ser Ala
 165 170 175

Phe Leu Arg Ala Gly Glu Asn Arg Leu Ala Val Met Val Leu Arg Trp
 180 185 190

50 Ser Asp Gly Ser Tyr Leu Glu Asp Gln Asp Met Trp Arg Met Ser Gly
 195 200 205

55 Ile Phe Arg Asp Val Ser Leu Leu His Lys Pro Thr Thr Gln Ile Ser
 210 215 220

Asp Phe His Val Ala Thr Arg Phe Asn Asp Asp Phe Ser Arg Ala Val
 225 230 235 240

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Leu Glu Ala Glu Val Gln Met Cys Gly Glu Leu Arg Asp Tyr Leu Arg
 245 250 255
 5 Val Thr Val Ser Leu Trp Gln Gly Glu Thr Gln Val Ala Ser Gly Thr
 260 265 270
 Ala Pro Phe Gly Gly Glu Ile Ile Asp Glu Arg Gly Gly Tyr Ala Asp
 275 280 285
 10 Arg Val Thr Leu Arg Leu Asn Val Glu Asn Pro Lys Leu Trp Ser Ala
 290 295 300
 Glu Ile Pro Asn Leu Tyr Arg Ala Val Val Glu Leu His Thr Ala Asp
 305 310 315 320
 15 Gly Thr Leu Ile Glu Ala Glu Ala Cys Asp Val Gly Phe Arg Glu Val
 325 330 335
 Arg Ile Glu Asn Gly Leu Leu Leu Leu Asn Gly Lys Pro Leu Leu Ile
 340 345 350
 Arg Gly Val Asn Arg His Glu His His Pro Leu His Gly Gln Val Met
 355 360 365
 25 Asp Glu Gln Thr Met Val Gln Asp Ile Leu Leu Met Lys Gln Asn Asn
 370 375 380
 Phe Asn Ala Val Arg Cys Ser His Tyr Pro Asn His Pro Leu Trp Tyr
 385 390 395 400
 30 Thr Leu Cys Asp Arg Tyr Gly Leu Tyr Val Val Asp Glu Ala Asn Ile
 405 410 415
 Glu Thr His Gly Met Val Pro Met Asn Arg Leu Thr Asp Asp Pro Arg
 420 425 430
 Trp Leu Pro Ala Met Ser Glu Arg Val Thr Arg Met Val Gln Arg Asp
 435 440 445
 40 Arg Asn His Pro Ser Val Ile Ile Trp Ser Leu Gly Asn Glu Ser Gly
 450 455 460
 His Gly Ala Asn His Asp Ala Leu Tyr Arg Trp Ile Lys Ser Val Asp
 465 470 475 480
 Pro Ser Arg Pro Val Gln Tyr Glu Gly Gly Gly Ala Asp Thr Thr Ala
 485 490 495
 50 Thr Asp Ile Ile Cys Pro Met Tyr Ala Arg Val Asp Glu Asp Gln Pro
 500 505 510
 Phe Pro Ala Val Pro Lys Trp Ser Ile Lys Lys Trp Leu Ser Leu Pro
 515 520 525
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Gly Glu Thr Arg Pro Leu Ile Leu Cys Glu Tyr Ala His Ala Met Gly
 530 535 540
 5
 Asn Ser Leu Gly Gly Phe Ala Lys Tyr Trp Gln Ala Phe Arg Gln Tyr
 545 550 555 560
 Pro Arg Leu Gln Gly Gly Phe Val Trp Asp Trp Val Asp Gln Ser Leu
 565 570 575
 10
 Ile Lys Tyr Asp Glu Asn Gly Asn Pro Trp Ser Ala Tyr Gly Gly Asp
 580 585 590
 Phe Gly Asp Thr Pro Asn Asp Arg Gln Phe Cys Met Asn Gly Leu Val
 595 600 605
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 Phe Ala Asp Arg Thr Pro His Pro Ala Leu Thr Glu Ala Lys His Gln
 610 615 620
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 Gln Gln Phe Phe Gln Phe Arg Leu Ser Gly Gln Thr Ile Glu Val Thr
 625 630 635 640
 Ser Glu Tyr Leu Phe Arg His Ser Asp Asn Glu Leu Leu His Trp Met
 645 650 655
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 Val Ala Leu Asp Gly Lys Pro Leu Ala Ser Gly Glu Val Pro Leu Asp
 660 665 670
 Val Ala Pro Gln Gly Lys Gln Leu Ile Glu Leu Pro Glu Leu Pro Gln
 675 680 685
 30
 Pro Glu Ser Ala Gly Gln Leu Trp Leu Thr Val Arg Val Val Gln Pro
 690 695 700
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 Asn Ala Thr Ala Trp Ser Glu Ala Gly His Ile Ser Ala Trp Gln Gln
 705 710 715 720
 Trp Arg Leu Ala Glu Asn Leu Ser Val Thr Leu Pro Ala Ala Ser His
 725 730 735
 40
 Ala Ile Pro His Leu Thr Thr Ser Glu Met Asp Phe Cys Ile Glu Leu
 740 745 750
 45
 Gly Asn Lys Arg Trp Gln Phe Asn Arg Gln Ser Gly Phe Leu Ser Gln
 755 760 765
 Met Trp Ile Gly Asp Lys Lys Gln Leu Leu Thr Pro Leu Arg Asp Gln
 770 775 780
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 Phe Thr Arg Ala Pro Leu Asp Asn Asp Ile Gly Val Ser Glu Ala Thr
 785 790 795 800
 Arg Ile Asp Pro Asn Ala Trp Val Glu Arg Trp Lys Ala Ala Gly His
 805 810 815
 55

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Tyr Gln Ala Glu Ala Ala Leu Leu Gln Cys Thr Ala Asp Thr Leu Ala
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 5 Asp Ala Val Leu Ile Thr Thr Ala His Ala Trp Gln His Gln Gly Lys
 835 840 845
 Thr Leu Phe Ile Ser Arg Lys Thr Tyr Arg Ile Asp Gly Ser Gly Gln
 850 855 860
 10 Met Ala Ile Thr Val Asp Val Glu Val Ala Ser Asp Thr Pro His Pro
 865 870 875 880
 Ala Arg Ile Gly Leu Asn Cys Gln Leu Ala Gln Val Ala Glu Arg Val
 885 890 895
 15 Asn Trp Leu Gly Leu Gly Pro Gln Glu Asn Tyr Pro Asp Arg Leu Thr
 900 905 910
 20 Ala Ala Cys Phe Asp Arg Trp Asp Leu Pro Leu Ser Asp Met Tyr Thr
 915 920 925
 Pro Tyr Val Phe Pro Ser Glu Asn Gly Leu Arg Cys Gly Thr Arg Glu
 930 935 940
 25 Leu Asn Tyr Gly Pro His Gln Trp Arg Gly Asp Phe Gln Phe Asn Ile
 945 950 955 960
 Ser Arg Tyr Ser Gln Gln Gln Leu Met Glu Thr Ser His Arg His Leu
 965 970 975
 30 Leu His Ala Glu Glu Gly Thr Trp Leu Asn Ile Asp Gly Phe His Met
 980 985 990
 Gly Ile Gly Gly Asp Asp Ser Trp Ser Pro Ser Val Ser Ala Glu Phe
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 55 Gly Ala Ile Ser Leu Ile Phe Ser Leu Lys Glu Glu Val Gly Ala Leu
 35 40 45

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Ala Lys Val Leu Arg Leu Phe Glu Glu Asn Asp Val Asn Leu Thr His
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5 Ile Glu Ser Arg Pro Ser Arg Leu Lys Lys Asp Glu Tyr Glu Phe Phe
65 70 75 80

Thr His Leu Asp Lys Arg Ser Leu Pro Ala Leu Thr Asn Ile Ile Lys
85 90 95

10 Ile Leu Arg His Asp Ile Gly Ala Thr Val His Glu Leu Ser Arg Asp
100 105 110

Lys Lys Lys Asp Thr Val Pro Trp Phe Pro Arg Thr Ile Gln Glu Leu
115 120 125

15 Asp Arg Phe Ala Asn Gln Ile Leu Ser Tyr Gly Ala Glu Leu Asp Ala
130 135 140

20 Asp His Pro Gly Phe Lys Asp Pro Val Tyr Arg Ala Arg Arg Lys Gln
145 150 155 160

Phe Ala Asp Ile Ala Tyr Asn Tyr Arg His Gly Gln Pro Ile Pro Arg
165 170 175

25 Val Glu Tyr Met Glu Glu Glu Lys Lys Thr Trp Gly Thr Val Phe Lys
180 185 190

30 Thr Leu Lys Ser Leu Tyr Lys Thr His Ala Cys Tyr Glu Tyr Asn His
195 200 205

Ile Phe Pro Leu Leu Glu Lys Tyr Cys Gly Phe His Glu Asp Asn Ile
210 215 220

35 Pro Gln Leu Glu Asp Val Ser Gln Phe Leu Gln Thr Cys Thr Gly Phe
225 230 235 240

Arg Leu Arg Pro Val Ala Gly Leu Leu Ser Ser Arg Asp Phe Leu Gly
245 250 255

40 Gly Leu Ala Phe Arg Val Phe His Cys Thr Gln Tyr Ile Arg His Gly
260 265 270

Ser Lys Pro Met Tyr Thr Pro Glu Pro Asp Ile Cys His Glu Leu Leu
275 280 285

Gly His Val Pro Leu Phe Ser Asp Arg Ser Phe Ala Gln Phe Ser Gln
290 295 300

50 Glu Ile Gly Leu Ala Ser Leu Gly Ala Pro Asp Glu Tyr Ile Glu Lys
305 310 315 320

Leu Ala Thr Ile Tyr Trp Phe Thr Val Glu Phe Gly Leu Cys Lys Gln
325 330 335

55

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Gly Asp Ser Ile Lys Ala Tyr Gly Ala Gly Leu Leu Ser Ser Phe Gly
 340 345 350
 5
 Glu Leu Gln Tyr Cys Leu Ser Glu Lys Pro Lys Leu Leu Pro Leu Glu
 355 360 365
 Leu Glu Lys Thr Ala Ile Gln Asn Tyr Thr Val Thr Glu Phe Gln Pro
 370 375 380
 10
 Leu Tyr Tyr Val Ala Glu Ser Phe Asn Asp Ala Lys Glu Lys Val Arg
 385 390 395 400
 Asn Phe Ala Ala Thr Ile Pro Arg Pro Phe Ser Val Arg Tyr Asp Pro
 405 410 415
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 Tyr Thr Gln Arg Ile Glu Val Leu Asp Asn Thr Gln Gln Leu Lys Ile
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 Gln Lys Ile Lys
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 Phe Ser Asp Leu Gln Asp Gly Arg Arg Leu Leu Asp Leu Leu Glu Gly
 35 40 45
 Leu Thr Gly Gln Lys Leu Pro Lys Glu Lys Gly Ser Thr Arg Val His
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 Ala Leu Asn Asn Val Asn Lys Ala Leu Arg Val Leu Gln Asn Asn Asn
 65 70 75 80
 Val Asp Leu Val Asn Ile Gly Ser Thr Asp Ile Val Asp Gly Asn His
 85 90 95
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 Lys Leu Thr Leu Gly Leu Ile Trp Asn Ile Ile Leu His Trp Gln Val
 100 105 110
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 Lys Asn Val Met Lys Asn Ile Met Ala Gly Leu Gln Gln Thr Asn Ser
 115 120 125
 Glu Lys Ile Leu Leu Ser Trp Val Arg Gln Ser Thr Arg Asn Tyr Pro

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Lys Gln Ser Asn Leu His Arg Val Leu Met Asp Leu Gln Asn Gln Lys
 435 440 445
 5
 Leu Lys Glu Leu Asn Asp Trp Leu Thr Lys Thr Glu Glu Arg Thr Arg
 450 455 460
 Lys Met Glu Glu Glu Pro Leu Gly Pro Asp Leu Glu Asp Leu Lys Arg
 465 470 475 480
 10
 Gln Val Gln Gln His Lys Val Leu Gln Glu Asp Leu Glu Gln Glu Gln
 485 490 495
 Val Arg Val Asn Ser Leu Thr His Met Val Val Val Val Asp Glu Ser
 500 505 510
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 Ser Gly Asp His Ala Thr Ala Ala Leu Glu Glu Gln Leu Lys Val Leu
 515 520 525
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 Gly Asp Arg Trp Ala Asn Ile Cys Arg Trp Thr Glu Asp Arg Trp Val
 530 535 540
 Leu Leu Gln Asp Ile Leu Leu Lys Trp Gln Arg Leu Thr Glu Glu Gln
 545 550 555 560
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 Cys Leu Phe Ser Ala Trp Leu Ser Glu Lys Glu Asp Ala Val Asn Lys
 565 570 575
 Ile His Thr Thr Gly Phe Lys Asp Gln Asn Glu Met Leu Ser Ser Leu
 580 585 590
 30
 Gln Lys Leu Ala Val Leu Lys Ala Asp Leu Glu Lys Lys Lys Gln Ser
 595 600 605
 35
 Met Gly Lys Leu Tyr Ser Leu Lys Gln Asp Leu Leu Ser Thr Leu Lys
 610 615 620
 Asn Lys Ser Val Thr Gln Lys Thr Glu Ala Trp Leu Asp Asn Phe Ala
 625 630 635 640
 40
 Arg Cys Trp Asp Asn Leu Val Gln Lys Leu Glu Lys Ser Thr Ala Gln
 645 650 655
 Ile Ser Gln Ala Val Thr Thr Thr Gln Pro Ser Leu Thr Gln Thr Thr
 660 665 670
 45
 Val Met Glu Thr Val Thr Thr Val Thr Thr Arg Glu Gln Ile Leu Val
 675 680 685
 50
 Lys His Ala Gln Glu Glu Leu Pro Pro Pro Pro Pro Gln Lys Lys Arg
 690 695 700
 Gln Ile Thr Val Asp Ser Glu Ile Arg Lys Arg Leu Asp Val Asp Ile
 705 710 715 720
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Thr Glu Leu His Ser Trp Ile Thr Arg Ser Glu Ala Val Leu Gln Ser
 725 730 735
 5 Pro Glu Phe Ala Ile Phe Arg Lys Glu Gly Asn Phe Ser Asp Leu Lys
 740 745 750
 Glu Lys Val Asn Ala Ile Glu Arg Glu Lys Ala Glu Lys Phe Arg Lys
 755 760 765
 10 Leu Gln Asp Ala Ser Arg Ser Ala Gln Ala Leu Val Glu Gln Met Val
 770 775 780
 Asn Glu Gly Val Asn Ala Asp Ser Ile Lys Gln Ala Ser Glu Gln Leu
 785 790 795 800
 15 Asn Ser Arg Trp Ile Glu Phe Cys Gln Leu Leu Ser Glu Arg Leu Asn
 805 810 815
 20 Trp Leu Glu Tyr Gln Asn Asn Ile Ile Ala Phe Tyr Asn Gln Leu Gln
 820 825 830
 Gln Leu Glu Gln Met Thr Thr Thr Ala Glu Asn Trp Leu Lys Ile Gln
 835 840 845
 25 Pro Thr Thr Pro Ser Glu Pro Thr Ala Ile Lys Ser Gln Leu Lys Ile
 850 855 860
 30 Cys Lys Asp Glu Val Asn Arg Leu Ser Gly Leu Gln Pro Gln Ile Glu
 865 870 875 880
 Arg Leu Lys Ile Gln Ser Ile Ala Leu Lys Glu Lys Gly Gln Gly Pro
 885 890 895
 35 Met Phe Leu Asp Ala Asp Phe Val Ala Phe Thr Asn His Phe Lys Gln
 900 905 910
 Val Phe Ser Asp Val Gln Ala Arg Glu Lys Glu Leu Gln Thr Ile Phe
 915 920 925
 40 Asp Thr Leu Pro Pro Met Arg Tyr Gln Glu Thr Met Ser Ala Ile Arg
 930 935 940
 Thr Trp Val Gln Gln Ser Glu Thr Lys Leu Ser Ile Pro Gln Leu Ser
 945 950 955 960
 Val Thr Asp Tyr Glu Ile Met Glu Gln Arg Leu Gly Glu Leu Gln Ala
 965 970 975
 50 Leu Gln Ser Ser Leu Gln Glu Gln Gln Ser Gly Leu Tyr Tyr Leu Ser
 980 985 990
 Thr Thr Val Lys Glu Met Ser Lys Lys Ala Pro Ser Glu Ile Ser Arg
 995 1000 1005
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Lys Tyr Gln Ser Glu Phe Glu Glu Ile Glu Gly Arg Trp Lys Lys
 1010 1015 1020
 5
 Leu Ser Ser Gln Leu Val Glu His Cys Gln Lys Leu Glu Glu Gln
 1025 1030 1035
 Met Asn Lys Leu Arg Lys Ile Gln Asn His Ile Gln Thr Leu Lys
 1040 1045 1050
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 Lys Trp Met Ala Glu Val Asp Val Phe Leu Lys Glu Glu Trp Pro
 1055 1060 1065
 Ala Leu Gly Asp Ser Glu Ile Leu Lys Lys Gln Leu Lys Gln Cys
 1070 1075 1080
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 Arg Leu Leu Val Ser Asp Ile Gln Thr Ile Gln Pro Ser Leu Asn
 1085 1090 1095
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 Ser Val Asn Glu Gly Gly Gln Lys Ile Lys Asn Glu Ala Glu Pro
 1100 1105 1110
 Glu Phe Ala Ser Arg Leu Glu Thr Glu Leu Lys Glu Leu Asn Thr
 1115 1120 1125
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 Gln Trp Asp His Met Cys Gln Gln Val Tyr Ala Arg Lys Glu Ala
 1130 1135 1140
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 Leu Lys Gly Gly Leu Glu Lys Thr Val Ser Leu Gln Lys Asp Leu
 1145 1150 1155
 Ser Glu Met His Glu Trp Met Thr Gln Ala Glu Glu Glu Tyr Leu
 1160 1165 1170
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 Glu Arg Asp Phe Glu Tyr Lys Thr Pro Asp Glu Leu Gln Lys Ala
 1175 1180 1185
 Val Glu Glu Met Lys Arg Ala Lys Glu Glu Ala Gln Gln Lys Glu
 1190 1195 1200
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 Ala Lys Val Lys Leu Leu Thr Glu Ser Val Asn Ser Val Ile Ala
 1205 1210 1215
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 Gln Ala Pro Pro Val Ala Gln Glu Ala Leu Lys Lys Glu Leu Glu
 1220 1225 1230
 Thr Leu Thr Thr Asn Tyr Gln Trp Leu Cys Thr Arg Leu Asn Gly
 1235 1240 1245
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 Lys Cys Lys Thr Leu Glu Glu Val Trp Ala Cys Trp His Glu Leu
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 Leu Ser Tyr Leu Glu Lys Ala Asn Lys Trp Leu Asn Glu Val Glu
 1265 1270 1275
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 Phe Lys Leu Lys Thr Thr Glu Asn Ile Pro Gly Gly Ala Glu Glu

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	Leu	Ser	Arg	Lys	Met	Arg	Lys	Glu	Met	Asn	Val	Leu	Thr	Glu	Trp
	1565						1570					1575			
5	Leu	Ala	Ala	Thr	Asp	Met	Glu	Leu	Thr	Lys	Arg	Ser	Ala	Val	Glu
	1580						1585					1590			
	Gly	Met	Pro	Ser	Asn	Leu	Asp	Ser	Glu	Val	Ala	Trp	Gly	Lys	Ala
	1595						1600					1605			
10	Thr	Gln	Lys	Glu	Ile	Glu	Lys	Gln	Lys	Val	His	Leu	Lys	Ser	Ile
	1610						1615					1620			
	Thr	Glu	Val	Gly	Glu	Ala	Leu	Lys	Thr	Val	Leu	Gly	Lys	Lys	Glu
15	1625						1630					1635			
	Thr	Leu	Val	Glu	Asp	Lys	Leu	Ser	Leu	Leu	Asn	Ser	Asn	Trp	Ile
	1640						1645					1650			
20	Ala	Val	Thr	Ser	Arg	Ala	Glu	Glu	Trp	Leu	Asn	Leu	Leu	Leu	Glu
	1655						1660					1665			
	Tyr	Gln	Lys	His	Met	Glu	Thr	Phe	Asp	Gln	Asn	Val	Asp	His	Ile
	1670						1675					1680			
25	Thr	Lys	Trp	Ile	Ile	Gln	Ala	Asp	Thr	Leu	Leu	Asp	Glu	Ser	Glu
	1685						1690					1695			
	Lys	Lys	Lys	Pro	Gln	Gln	Lys	Glu	Asp	Val	Leu	Lys	Arg	Leu	Lys
30	1700						1705					1710			
	Ala	Glu	Leu	Asn	Asp	Ile	Arg	Pro	Lys	Val	Asp	Ser	Thr	Arg	Asp
	1715						1720					1725			
35	Gln	Ala	Ala	Asn	Leu	Met	Ala	Asn	Arg	Gly	Asp	His	Cys	Arg	Lys
	1730						1735					1740			
	Leu	Val	Glu	Pro	Gln	Ile	Ser	Glu	Leu	Asn	His	Arg	Phe	Ala	Ala
	1745						1750					1755			
40	Ile	Ser	His	Arg	Ile	Lys	Thr	Gly	Lys	Ala	Ser	Ile	Pro	Leu	Lys
	1760						1765					1770			
	Glu	Leu	Glu	Gln	Phe	Asn	Ser	Asp	Ile	Gln	Lys	Leu	Leu	Glu	Pro
45	1775						1780					1785			
	Leu	Glu	Ala	Glu	Ile	Gln	Gln	Gly	Val	Asn	Leu	Lys	Glu	Glu	Asp
	1790						1795					1800			
50	Phe	Asn	Lys	Asp	Met	Asn	Glu	Asp	Asn	Glu	Gly	Thr	Val	Lys	Glu
	1805						1810					1815			
	Leu	Leu	Gln	Arg	Gly	Asp	Asn	Leu	Gln	Gln	Arg	Ile	Thr	Asp	Glu
55	1820						1825					1830			

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	Arg	Lys	Arg	Glu	Glu	Ile	Lys	Ile	Lys	Gln	Gln	Leu	Leu	Gln	Thr
	1835						1840					1845			
5	Lys	His	Asn	Ala	Leu	Lys	Asp	Leu	Arg	Ser	Gln	Arg	Arg	Lys	Lys
	1850						1855					1860			
	Ala	Leu	Glu	Ile	Ser	His	Gln	Trp	Tyr	Gln	Tyr	Lys	Arg	Gln	Ala
	1865						1870					1875			
10	Asp	Asp	Leu	Leu	Lys	Cys	Leu	Asp	Asp	Ile	Glu	Lys	Lys	Leu	Ala
	1880						1885					1890			
	Ser	Leu	Pro	Glu	Pro	Arg	Asp	Glu	Arg	Lys	Ile	Lys	Glu	Ile	Asp
15	1895						1900					1905			
	Arg	Glu	Leu	Gln	Lys	Lys	Lys	Glu	Glu	Leu	Asn	Ala	Val	Arg	Arg
	1910						1915					1920			
20	Gln	Ala	Glu	Gly	Leu	Ser	Glu	Asp	Gly	Ala	Ala	Met	Ala	Val	Glu
	1925						1930					1935			
	Pro	Thr	Gln	Ile	Gln	Leu	Ser	Lys	Arg	Trp	Arg	Glu	Ile	Glu	Ser
	1940						1945					1950			
25	Lys	Phe	Ala	Gln	Phe	Arg	Arg	Leu	Asn	Phe	Ala	Gln	Ile	His	Thr
	1955						1960					1965			
	Val	Arg	Glu	Glu	Thr	Met	Met	Val	Met	Thr	Glu	Asp	Met	Pro	Leu
30	1970						1975					1980			
	Glu	Ile	Ser	Tyr	Val	Pro	Ser	Thr	Tyr	Leu	Thr	Glu	Ile	Thr	His
	1985						1990					1995			
35	Val	Ser	Gln	Ala	Leu	Leu	Glu	Val	Glu	Gln	Leu	Leu	Asn	Ala	Pro
	2000						2005					2010			
	Asp	Leu	Cys	Ala	Lys	Asp	Phe	Glu	Asp	Leu	Phe	Lys	Gln	Glu	Glu
40	2015						2020					2025			
	Ser	Leu	Lys	Asn	Ile	Lys	Asp	Ser	Leu	Gln	Gln	Ser	Ser	Gly	Arg
	2030						2035					2040			
45	Ile	Asp	Ile	Ile	His	Ser	Lys	Lys	Thr	Ala	Ala	Leu	Gln	Ser	Ala
	2045						2050					2055			
	Thr	Pro	Val	Glu	Arg	Val	Lys	Leu	Gln	Glu	Ala	Leu	Ser	Gln	Leu
	2060						2065					2070			
50	Asp	Phe	Gln	Trp	Glu	Lys	Val	Asn	Lys	Met	Tyr	Lys	Asp	Arg	Gln
	2075						2080					2085			
	Gly	Arg	Phe	Asp	Arg	Ser	Val	Glu	Lys	Trp	Arg	Arg	Phe	His	Tyr
55	2090						2095					2100			

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Asp Ile Lys Ile Phe Asn Gln Trp Leu Thr Glu Ala Glu Gln Phe
 2105 2110 2115
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 Leu Arg Lys Thr Gln Ile Pro Glu Asn Trp Glu His Ala Lys Tyr
 2120 2125 2130
 Lys Trp Tyr Leu Lys Glu Leu Gln Asp Gly Ile Gly Gln Arg Gln
 2135 2140 2145
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 Thr Val Val Arg Thr Leu Asn Ala Thr Gly Glu Glu Ile Ile Gln
 2150 2155 2160
 Gln Ser Ser Lys Thr Asp Ala Ser Ile Leu Gln Glu Lys Leu Gly
 2165 2170 2175
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 Ser Leu Asn Leu Arg Trp Gln Glu Val Cys Lys Gln Leu Ser Asp
 2180 2185 2190
 Arg Lys Lys Arg Leu Glu Glu Gln Lys Asn Ile Leu Ser Glu Phe
 2195 2200 2205
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 Gln Arg Asp Leu Asn Glu Phe Val Leu Trp Leu Glu Glu Ala Asp
 2210 2215 2220
 25
 Asn Ile Ala Ser Ile Pro Leu Glu Pro Gly Lys Glu Gln Gln Leu
 2225 2230 2235
 Lys Glu Lys Leu Glu Gln Val Lys Leu Leu Val Glu Glu Leu Pro
 2240 2245 2250
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 Leu Arg Gln Gly Ile Leu Lys Gln Leu Asn Glu Thr Gly Gly Pro
 2255 2260 2265
 Val Leu Val Ser Ala Pro Ile Ser Pro Glu Glu Gln Asp Lys Leu
 2270 2275 2280
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 Glu Asn Lys Leu Lys Gln Thr Asn Leu Gln Trp Ile Lys Val Ser
 2285 2290 2295
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 Arg Ala Leu Pro Glu Lys Gln Gly Glu Ile Glu Ala Gln Ile Lys
 2300 2305 2310
 Asp Leu Gly Gln Leu Glu Lys Lys Leu Glu Asp Leu Glu Glu Gln
 2315 2320 2325
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 Leu Asn His Leu Leu Leu Trp Leu Ser Pro Ile Arg Asn Gln Leu
 2330 2335 2340
 Glu Ile Tyr Asn Gln Pro Asn Gln Glu Gly Pro Phe Asp Val Gln
 2345 2350 2355
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 Glu Thr Glu Ile Ala Val Gln Ala Lys Gln Pro Asp Val Glu Glu
 2360 2365 2370
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 Ile Leu Ser Lys Gly Gln His Leu Tyr Lys Glu Lys Pro Ala Thr

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	2375		2380		2385
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	Ala Val Asn Arg Leu Leu Gln Glu Leu Arg Ala Lys Gln Pro Asp 2405 2410 2415				
10	Leu Ala Pro Gly Leu Thr Thr Ile Gly Ala Ser Pro Thr Gln Thr 2420 2425 2430				
	Val Thr Leu Val Thr Gln Pro Val Val Thr Lys Glu Thr Ala Ile 2435 2440 2445				
15	Ser Lys Leu Glu Met Pro Ser Ser Leu Met Leu Glu Val Pro Ala 2450 2455 2460				
	Leu Ala Asp Phe Asn Arg Ala Trp Thr Glu Leu Thr Asp Trp Leu 2465 2470 2475				
20	Ser Leu Leu Asp Gln Val Ile Lys Ser Gln Arg Val Met Val Gly 2480 2485 2490				
	Asp Leu Glu Asp Ile Asn Glu Met Ile Ile Lys Gln Lys Ala Thr 2495 2500 2505				
25	Met Gln Asp Leu Glu Gln Arg Arg Pro Gln Leu Glu Glu Leu Ile 2510 2515 2520				
30	Thr Ala Ala Gln Asn Leu Lys Asn Lys Thr Ser Asn Gln Glu Ala 2525 2530 2535				
	Arg Thr Ile Ile Thr Asp Arg Ile Glu Arg Ile Gln Asn Gln Trp 2540 2545 2550				
35	Asp Glu Val Gln Glu His Leu Gln Asn Arg Arg Gln Gln Leu Asn 2555 2560 2565				
	Glu Met Leu Lys Asp Ser Thr Gln Trp Leu Glu Ala Lys Glu Glu 2570 2575 2580				
40	Ala Glu Gln Val Leu Gly Gln Ala Arg Ala Lys Leu Glu Ser Trp 2585 2590 2595				
45	Lys Glu Gly Pro Tyr Thr Val Asp Ala Ile Gln Lys Lys Ile Thr 2600 2605 2610				
	Glu Thr Lys Gln Leu Ala Lys Asp Leu Arg Gln Trp Gln Thr Asn 2615 2620 2625				
50	Val Asp Val Ala Asn Asp Leu Ala Leu Lys Leu Leu Arg Asp Tyr 2630 2635 2640				
55	Ser Ala Asp Asp Thr Arg Lys Val His Met Ile Thr Glu Asn Ile 2645 2650 2655				

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	Asn	Ala	Ser	Trp	Arg	Ser	Ile	His	Lys	Arg	Val	Ser	Glu	Arg	Glu
	2660						2665					2670			
5	Ala	Ala	Leu	Glu	Glu	Thr	His	Arg	Leu	Leu	Gln	Gln	Phe	Pro	Leu
	2675						2680					2685			
	Asp	Leu	Glu	Lys	Phe	Leu	Ala	Trp	Leu	Thr	Glu	Ala	Glu	Thr	Thr
	2690						2695					2700			
10	Ala	Asn	Val	Leu	Gln	Asp	Ala	Thr	Arg	Lys	Glu	Arg	Leu	Leu	Glu
	2705						2710					2715			
	Asp	Ser	Lys	Gly	Val	Lys	Glu	Leu	Met	Lys	Gln	Trp	Gln	Asp	Leu
	2720						2725					2730			
15	Gln	Gly	Glu	Ile	Glu	Ala	His	Thr	Asp	Val	Tyr	His	Asn	Leu	Asp
	2735						2740					2745			
	Glu	Asn	Ser	Gln	Lys	Ile	Leu	Arg	Ser	Leu	Glu	Gly	Ser	Asp	Asp
	2750						2755					2760			
20	Ala	Val	Leu	Leu	Gln	Arg	Arg	Leu	Asp	Asn	Met	Asn	Phe	Lys	Trp
	2765						2770					2775			
25	Ser	Glu	Leu	Arg	Lys	Lys	Ser	Leu	Asn	Ile	Arg	Ser	His	Leu	Glu
	2780						2785					2790			
	Ala	Ser	Ser	Asp	Gln	Trp	Lys	Arg	Leu	His	Leu	Ser	Leu	Gln	Glu
	2795						2800					2805			
30	Leu	Leu	Val	Trp	Leu	Gln	Leu	Lys	Asp	Asp	Glu	Leu	Ser	Arg	Gln
	2810						2815					2820			
	Ala	Pro	Ile	Gly	Gly	Asp	Phe	Pro	Ala	Val	Gln	Lys	Gln	Asn	Asp
	2825						2830					2835			
35	Val	His	Arg	Ala	Phe	Lys	Arg	Glu	Leu	Lys	Thr	Lys	Glu	Pro	Val
	2840						2845					2850			
40	Ile	Met	Ser	Thr	Leu	Glu	Thr	Val	Arg	Ile	Phe	Leu	Thr	Glu	Gln
	2855						2860					2865			
	Pro	Leu	Glu	Gly	Leu	Glu	Lys	Leu	Tyr	Gln	Glu	Pro	Arg	Glu	Leu
	2870						2875					2880			
45	Pro	Pro	Glu	Glu	Arg	Ala	Gln	Asn	Val	Thr	Arg	Leu	Leu	Arg	Lys
	2885						2890					2895			
	Gln	Ala	Glu	Glu	Val	Asn	Thr	Glu	Trp	Glu	Lys	Leu	Asn	Leu	His
	2900						2905					2910			
50	Ser	Ala	Asp	Trp	Gln	Arg	Lys	Ile	Asp	Glu	Thr	Leu	Glu	Arg	Leu
	2915						2920					2925			
55															

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Gln Glu Leu Gln Glu Ala Thr Asp Glu Leu Asp Leu Lys Leu Arg
 2930 2935 2940
 5
 Gln Ala Glu Val Ile Lys Gly Ser Trp Gln Pro Val Gly Asp Leu
 2945 2950 2955
 Leu Ile Asp Ser Leu Gln Asp His Leu Glu Lys Val Lys Ala Leu
 2960 2965 2970
 10
 Arg Gly Glu Ile Ala Pro Leu Lys Glu Asn Val Ser His Val Asn
 2975 2980 2985
 Asp Leu Ala Arg Gln Leu Thr Thr Leu Gly Ile Gln Leu Ser Pro
 2990 2995 3000
 15
 Tyr Asn Leu Ser Thr Leu Glu Asp Leu Asn Thr Arg Trp Lys Leu
 3005 3010 3015
 Leu Gln Val Ala Val Glu Asp Arg Val Arg Gln Leu His Glu Ala
 3020 3025 3030
 His Arg Asp Phe Gly Pro Ala Ser Gln His Phe Leu Ser Thr Ser
 3035 3040 3045
 25
 Val Gln Gly Pro Trp Glu Arg Ala Ile Ser Pro Asn Lys Val Pro
 3050 3055 3060
 Tyr Tyr Ile Asn His Glu Thr Gln Thr Thr Cys Trp Asp His Pro
 3065 3070 3075
 30
 Lys Met Thr Glu Leu Tyr Gln Ser Leu Ala Asp Leu Asn Asn Val
 3080 3085 3090
 Arg Phe Ser Ala Tyr Arg Thr Ala Met Lys Leu Arg Arg Leu Gln
 3095 3100 3105
 Lys Ala Leu Cys Leu Asp Leu Leu Ser Leu Ser Ala Ala Cys Asp
 3110 3115 3120
 40
 Ala Leu Asp Gln His Asn Leu Lys Gln Asn Asp Gln Pro Met Asp
 3125 3130 3135
 Ile Leu Gln Ile Ile Asn Cys Leu Thr Thr Ile Tyr Asp Arg Leu
 3140 3145 3150
 45
 Glu Gln Glu His Asn Asn Leu Val Asn Val Pro Leu Cys Val Asp
 3155 3160 3165
 Met Cys Leu Asn Trp Leu Leu Asn Val Tyr Asp Thr Gly Arg Thr
 3170 3175 3180
 50
 Gly Arg Ile Arg Val Leu Ser Phe Lys Thr Gly Ile Ile Ser Leu
 3185 3190 3195
 55

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	Cys	Lys	Ala	His	Leu	Glu	Asp	Lys	Tyr	Arg	Tyr	Leu	Phe	Lys	Gln
	3200						3205					3210			
5	Val	Ala	Ser	Ser	Thr	Gly	Phe	Cys	Asp	Gln	Arg	Arg	Leu	Gly	Leu
	3215						3220					3225			
	Leu	Leu	His	Asp	Ser	Ile	Gln	Ile	Pro	Arg	Gln	Leu	Gly	Glu	Val
10	3230						3235					3240			
	Ala	Ser	Phe	Gly	Gly	Ser	Asn	Ile	Glu	Pro	Ser	Val	Arg	Ser	Cys
	3245						3250					3255			
	Phe	Gln	Phe	Ala	Asn	Asn	Lys	Pro	Glu	Ile	Glu	Ala	Ala	Leu	Phe
15	3260						3265					3270			
	Leu	Asp	Trp	Met	Arg	Leu	Glu	Pro	Gln	Ser	Met	Val	Trp	Leu	Pro
	3275						3280					3285			
20	Val	Leu	His	Arg	Val	Ala	Ala	Ala	Glu	Thr	Ala	Lys	His	Gln	Ala
	3290						3295					3300			
	Lys	Cys	Asn	Ile	Cys	Lys	Glu	Cys	Pro	Ile	Ile	Gly	Phe	Arg	Tyr
25	3305						3310					3315			
	Arg	Ser	Leu	Lys	His	Phe	Asn	Tyr	Asp	Ile	Cys	Gln	Ser	Cys	Phe
	3320						3325					3330			
	Phe	Ser	Gly	Arg	Val	Ala	Lys	Gly	His	Lys	Met	His	Tyr	Pro	Met
30	3335						3340					3345			
	Val	Glu	Tyr	Cys	Thr	Pro	Thr	Thr	Ser	Gly	Glu	Asp	Val	Arg	Asp
	3350						3355					3360			
35	Phe	Ala	Lys	Val	Leu	Lys	Asn	Lys	Phe	Arg	Thr	Lys	Arg	Tyr	Phe
	3365						3370					3375			
	Ala	Lys	His	Pro	Arg	Met	Gly	Tyr	Leu	Pro	Val	Gln	Thr	Val	Leu
40	3380						3385					3390			
	Glu	Gly	Asp	Asn	Met	Glu	Thr	Pro	Val	Thr	Leu	Ile	Asn	Phe	Trp
	3395						3400					3405			
45	Pro	Val	Asp	Ser	Ala	Pro	Ala	Ser	Ser	Pro	Gln	Leu	Ser	His	Asp
	3410						3415					3420			
	Asp	Thr	His	Ser	Arg	Ile	Glu	His	Tyr	Ala	Ser	Arg	Leu	Ala	Glu
	3425						3430					3435			
50	Met	Glu	Asn	Ser	Asn	Gly	Ser	Tyr	Leu	Asn	Asp	Ser	Ile	Ser	Pro
	3440						3445					3450			
	Asn	Glu	Ser	Ile	Asp	Asp	Glu	His	Leu	Leu	Ile	Gln	His	Tyr	Cys
55	3455						3460					3465			
	Gln	Ser	Leu	Asn	Gln	Asp	Ser	Pro	Leu	Ser	Gln	Pro	Arg	Ser	Pro

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	3470		3475		3480								
5	Ala Gln	Ile Leu	Ile Ser	Leu	Glu Ser	Glu Glu	Arg	Gly Glu	Leu				
	3485			3490			3495						
	Glu Arg	Ile Leu	Ala Asp	Leu	Glu Glu	Glu Asn	Arg	Asn Leu	Gln				
	3500			3505			3510						
10	Ala Glu	Tyr Asp	Arg Leu	Lys	Gln Gln	His Glu	His	Lys Gly	Leu				
	3515			3520			3525						
	Ser Pro	Leu Pro	Ser Pro	Pro	Glu Met	Met Pro	Thr	Ser Pro	Gln				
15	3530			3535			3540						
	Ser Pro	Arg Asp	Ala Glu	Leu	Ile Ala	Glu Ala	Lys	Leu Leu	Arg				
	3545			3550			3555						
20	Gln His	Lys Gly	Arg Leu	Glu	Ala Arg	Met Gln	Ile	Leu Glu	Asp				
	3560			3565			3570						
	His Asn	Lys Gln	Leu Glu	Ser	Gln Leu	His Arg	Leu	Arg Gln	Leu				
	3575			3580			3585						
25	Leu Glu	Gln Pro	Gln Ala	Glu	Ala Lys	Val Asn	Gly	Thr Thr	Val				
	3590			3595			3600						
	Ser Ser	Pro Ser	Thr Ser	Leu	Gln Arg	Ser Asp	Ser	Ser Gln	Pro				
30	3605			3610			3615						
	Met Leu	Leu Arg	Val Val	Gly	Ser Gln	Thr Ser	Asp	Ser Met	Gly				
	3620			3625			3630						
35	Glu Glu	Asp Leu	Leu Ser	Pro	Pro Gln	Asp Thr	Ser	Thr Gly	Leu				
	3635			3640			3645						
	Glu Glu	Val Met	Glu Gln	Leu	Asn Asn	Ser Phe	Pro	Ser Ser	Arg				
	3650			3655			3660						
40	Gly Arg	Asn Thr	Pro Gly	Lys	Pro Met	Arg Glu	Asp	Thr Met					
	3665			3670			3675						

<210> 5

<211> 536

45 <212> PRT

<213> Homo sapiens

<400> 5

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55

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Met Glu Phe Ser Ser Pro Ser Arg Glu Glu Cys Pro Lys Pro Leu Ser
1 5 10 15

5 Arg Val Ser Ile Met Ala Gly Ser Leu Thr Gly Leu Leu Leu Leu Gln
20 25 30

Ala Val Ser Trp Ala Ser Gly Ala Arg Pro Cys Ile Pro Lys Ser Phe
35 40 45

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Gly Tyr Ser Ser Val Val Cys Val Cys Asn Ala Thr Tyr Cys Asp Ser
 50 55 60
 5 Phe Asp Pro Pro Thr Phe Pro Ala Leu Gly Thr Phe Ser Arg Tyr Glu
 65 70 75 80
 Ser Thr Arg Ser Gly Arg Arg Met Glu Leu Ser Met Gly Pro Ile Gln
 85 90 95
 10 Ala Asn His Thr Gly Thr Gly Leu Leu Leu Thr Leu Gln Pro Glu Gln
 100 105 110
 15 Lys Phe Gln Lys Val Lys Gly Phe Gly Gly Ala Met Thr Asp Ala Ala
 115 120 125
 Ala Leu Asn Ile Leu Ala Leu Ser Pro Pro Ala Gln Asn Leu Leu Leu
 130 135 140
 20 Lys Ser Tyr Phe Ser Glu Glu Gly Ile Gly Tyr Asn Ile Ile Arg Val
 145 150 155 160
 Pro Met Ala Ser Cys Asp Phe Ser Ile Arg Thr Tyr Thr Tyr Ala Asp
 165 170 175
 25 Thr Pro Asp Asp Phe Gln Leu His Asn Phe Ser Leu Pro Glu Glu Asp
 180 185 190
 30 Thr Lys Leu Lys Ile Pro Leu Ile His Arg Ala Leu Gln Leu Ala Gln
 195 200 205
 Arg Pro Val Ser Leu Leu Ala Ser Pro Trp Thr Ser Pro Thr Trp Leu
 210 215 220
 35 Lys Thr Asn Gly Ala Val Asn Gly Lys Gly Ser Leu Lys Gly Gln Pro
 225 230 235 240
 Gly Asp Ile Tyr His Gln Thr Trp Ala Arg Tyr Phe Val Lys Phe Leu
 245 250 255
 40 Asp Ala Tyr Ala Glu His Lys Leu Gln Phe Trp Ala Val Thr Ala Glu
 260 265 270
 45 Asn Glu Pro Ser Ala Gly Leu Leu Ser Gly Tyr Pro Phe Gln Cys Leu
 275 280 285
 Gly Phe Thr Pro Glu His Gln Arg Asp Phe Ile Ala Arg Asp Leu Gly
 290 295 300
 50 Pro Thr Leu Ala Asn Ser Thr His His Asn Val Arg Leu Leu Met Leu
 305 310 315 320
 Asp Asp Gln Arg Leu Leu Leu Pro His Trp Ala Lys Val Val Leu Thr
 325 330 335
 55

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Asp Pro Glu Ala Ala Lys Tyr Val His Gly Ile Ala Val His Trp Tyr
 340 345 350

5

 Leu Asp Phe Leu Ala Pro Ala Lys Ala Thr Leu Gly Glu Thr His Arg
 355 360 365

Leu Phe Pro Asn Thr Met Leu Phe Ala Ser Glu Ala Cys Val Gly Ser
 370 375 380

10

 Lys Phe Trp Glu Gln Ser Val Arg Leu Gly Ser Trp Asp Arg Gly Met
 385 390 395 400

Gln Tyr Ser His Ser Ile Ile Thr Asn Leu Leu Tyr His Val Val Gly
 405 410 415

15

 Trp Thr Asp Trp Asn Leu Ala Leu Asn Pro Glu Gly Gly Pro Asn Trp
 420 425 430

20

 Val Arg Asn Phe Val Asp Ser Pro Ile Ile Val Asp Ile Thr Lys Asp
 435 440 445

Thr Phe Tyr Lys Gln Pro Met Phe Tyr His Leu Gly His Phe Ser Lys
 450 455 460

25

 Phe Ile Pro Glu Gly Ser Gln Arg Val Gly Leu Val Ala Ser Gln Lys
 465 470 475 480

Asn Asp Leu Asp Ala Val Ala Leu Met His Pro Asp Gly Ser Ala Val
 485 490 495

30

 Val Val Val Leu Asn Arg Ser Ser Lys Asp Val Pro Leu Thr Ile Lys
 500 505 510

35

 Asp Pro Ala Val Gly Phe Leu Glu Thr Ile Ser Pro Gly Tyr Ser Ile
 515 520 525

His Thr Tyr Leu Trp Arg Arg Gln
 530 535

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 <210> 6
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 <212> PRT
 <213> Homo sapiens

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 <400> 6

Met Ala Leu Trp Met Arg Leu Leu Pro Leu Leu Ala Leu Leu Ala Leu
 1 5 10 15

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 Trp Gly Pro Asp Pro Ala Ala Ala Phe Val Asn Gln His Leu Cys Gly
 20 25 30

Ser His Leu Val Glu Ala Leu Tyr Leu Val Cys Gly Glu Arg Gly Phe
 35 40 45

55

 Phe Tyr Thr Pro Lys Thr Arg Arg Glu Ala Glu Asp Leu Gln Val Gly
 50 55 60

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Gln Val Glu Leu Gly Gly Gly Pro Gly Ala Gly Ser Leu Gln Pro Leu
 65 70 75 80

Ala Leu Glu Gly Ser Leu Gln Lys Arg Gly Ile Val Glu Gln Cys Cys
 5 85 90 95

Thr Ser Ile Cys Ser Leu Tyr Gln Leu Glu Asn Tyr Cys Asn
 100 105 110

<210> 7
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 <212> PRT
 <213> Homo sapiens

<400> 7

Met Lys Ile Leu Ile Leu Gly Ile Phe Leu Phe Leu Cys Ser Thr Pro
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Ala Trp Ala Lys Glu Lys His Tyr Tyr Ile Gly Ile Ile Glu Thr Thr
 20 20 25 30

Trp Asp Tyr Ala Ser Asp His Gly Glu Lys Lys Leu Ile Ser Val Asp
 25 35 40 45

Thr Glu His Ser Asn Ile Tyr Leu Gln Asn Gly Pro Asp Arg Ile Gly
 50 55 60

Arg Leu Tyr Lys Lys Ala Leu Tyr Leu Gln Tyr Thr Asp Glu Thr Phe
 30 65 70 75 80

Arg Thr Thr Ile Glu Lys Pro Val Trp Leu Gly Phe Leu Gly Pro Ile
 85 90 95

Ile Lys Ala Glu Thr Gly Asp Lys Val Tyr Val His Leu Lys Asn Leu
 100 105 110

Ala Ser Arg Pro Tyr Thr Phe His Ser His Gly Ile Thr Tyr Tyr Lys
 40 115 120 125

Glu His Glu Gly Ala Ile Tyr Pro Asp Asn Thr Thr Asp Phe Gln Arg
 130 135 140

Ala Asp Asp Lys Val Tyr Pro Gly Glu Gln Tyr Thr Tyr Met Leu Leu
 45 145 150 155 160

Ala Thr Glu Glu Gln Ser Pro Gly Glu Gly Asp Gly Asn Cys Val Thr
 165 170 175

Arg Ile Tyr His Ser His Ile Asp Ala Pro Lys Asp Ile Ala Ser Gly
 180 185 190

Leu Ile Gly Pro Leu Ile Ile Cys Lys Lys Asp Ser Leu Asp Lys Glu
 55 195 200 205

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Lys Glu Lys His Ile Asp Arg Glu Phe Val Val Met Phe Ser Val Val
 210 215 220
 5 Asp Glu Asn Phe Ser Trp Tyr Leu Glu Asp Asn Ile Lys Thr Tyr Cys
 225 230 235 240
 Ser Glu Pro Glu Lys Val Asp Lys Asp Asn Glu Asp Phe Gln Glu Ser
 245 250 255
 10 Asn Arg Met Tyr Ser Val Asn Gly Tyr Thr Phe Gly Ser Leu Pro Gly
 260 265 270
 Leu Ser Met Cys Ala Glu Asp Arg Val Lys Trp Tyr Leu Phe Gly Met
 275 280 285
 15 Gly Asn Glu Val Asp Val His Ala Ala Phe Phe His Gly Gln Ala Leu
 290 295 300
 Thr Asn Lys Asn Tyr Arg Ile Asp Thr Ile Asn Leu Phe Pro Ala Thr
 305 310 315 320
 Leu Phe Asp Ala Tyr Met Val Ala Gln Asn Pro Gly Glu Trp Met Leu
 325 330 335
 25 Ser Cys Gln Asn Leu Asn His Leu Lys Ala Gly Leu Gln Ala Phe Phe
 340 345 350
 Gln Val Gln Glu Cys Asn Lys Ser Ser Ser Lys Asp Asn Ile Arg Gly
 355 360 365
 30 Lys His Val Arg His Tyr Tyr Ile Ala Ala Glu Glu Ile Ile Trp Asn
 370 375 380
 Tyr Ala Pro Ser Gly Ile Asp Ile Phe Thr Lys Glu Asn Leu Thr Ala
 385 390 395 400
 Pro Gly Ser Asp Ser Ala Val Phe Phe Glu Gln Gly Thr Thr Arg Ile
 405 410 415
 40 Gly Gly Ser Tyr Lys Lys Leu Val Tyr Arg Glu Tyr Thr Asp Ala Ser
 420 425 430
 Phe Thr Asn Arg Lys Glu Arg Gly Pro Glu Glu Glu His Leu Gly Ile
 435 440 445
 Leu Gly Pro Val Ile Trp Ala Glu Val Gly Asp Thr Ile Arg Val Thr
 450 455 460
 50 Phe His Asn Lys Gly Ala Tyr Pro Leu Ser Ile Glu Pro Ile Gly Val
 465 470 475 480
 Arg Phe Asn Lys Asn Asn Glu Gly Thr Tyr Tyr Ser Pro Asn Tyr Asn
 485 490 495
 55 Pro Gln Ser Arg Ser Val Pro Pro Ser Ala Ser His Val Ala Pro Thr

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Glu Glu Glu His Leu Gly Ile Leu Gly Pro Gln Leu His Ala Asp Val
 805 810 815
 5 Gly Asp Lys Val Lys Ile Ile Phe Lys Asn Met Ala Thr Arg Pro Tyr
 820 825 830
 Ser Ile His Ala His Gly Val Gln Thr Glu Ser Ser Thr Val Thr Pro
 835 840 845
 10 Thr Leu Pro Gly Glu Thr Leu Thr Tyr Val Trp Lys Ile Pro Glu Arg
 850 855 860
 Ser Gly Ala Gly Thr Glu Asp Ser Ala Cys Ile Pro Trp Ala Tyr Tyr
 865 870 875 880
 15 Ser Thr Val Asp Gln Val Lys Asp Leu Tyr Ser Gly Leu Ile Gly Pro
 885 890 895
 20 Leu Ile Val Cys Arg Arg Pro Tyr Leu Lys Val Phe Asn Pro Arg Arg
 900 905 910
 Lys Leu Glu Phe Ala Leu Leu Phe Leu Val Phe Asp Glu Asn Glu Ser
 915 920 925
 25 Trp Tyr Leu Asp Asp Asn Ile Lys Thr Tyr Ser Asp His Pro Glu Lys
 930 935 940
 Val Asn Lys Asp Asp Glu Glu Phe Ile Glu Ser Asn Lys Met His Ala
 945 950 955 960
 30 Ile Asn Gly Arg Met Phe Gly Asn Leu Gln Gly Leu Thr Met His Val
 965 970 975
 Gly Asp Glu Val Asn Trp Tyr Leu Met Gly Met Gly Asn Glu Ile Asp
 980 985 990
 Leu His Thr Val His Phe His Gly His Ser Phe Gln Tyr Lys His Arg
 995 1000 1005
 40 Gly Val Tyr Ser Ser Asp Val Phe Asp Ile Phe Pro Gly Thr Tyr
 1010 1015 1020
 Gln Thr Leu Glu Met Phe Pro Arg Thr Pro Gly Ile Trp Leu Leu
 1025 1030 1035
 45 His Cys His Val Thr Asp His Ile His Ala Gly Met Glu Thr Thr
 1040 1045 1050
 Tyr Thr Val Leu Gln Asn Glu Asp Thr Lys Ser Gly
 1055 1060 1065
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<210> 8

<211> 471

55 <212> PRT

<213> Escherichia coli

<400> 8

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Met Lys Gln Ser Thr Ile Ala Leu Ala Leu Leu Pro Leu Leu Phe Thr
1 5 10 15

Pro Val Thr Lys Ala Arg Thr Pro Glu Met Pro Val Leu Glu Asn Arg
5 20 25 30

Ala Ala Gln Gly Asp Ile Thr Ala Pro Gly Gly Ala Arg Arg Leu Thr
35 40 45

Gly Asp Gln Thr Ala Ala Leu Arg Asp Ser Leu Ser Asp Lys Pro Ala
10 50 55 60

Lys Asn Ile Ile Leu Leu Ile Gly Asp Gly Met Gly Asp Ser Glu Ile
15 65 70 75 80

Thr Ala Ala Arg Asn Tyr Ala Glu Gly Ala Gly Gly Phe Phe Lys Gly
85 90 95

Ile Asp Ala Leu Pro Leu Thr Gly Gln Tyr Thr His Tyr Ala Leu Asn
20 100 105 110

Lys Lys Thr Gly Lys Pro Asp Tyr Val Thr Asp Ser Ala Ala Ser Ala
115 120 125

Thr Ala Trp Ser Thr Gly Val Lys Thr Tyr Asn Gly Ala Leu Gly Val
25 130 135 140

Asp Ile His Glu Lys Asp His Pro Thr Ile Leu Glu Met Ala Lys Ala
30 145 150 155 160

Ala Gly Leu Ala Thr Gly Asn Val Ser Thr Ala Glu Leu Gln Asp Ala
165 170 175

Thr Pro Ala Ala Leu Val Ala His Val Thr Ser Arg Lys Cys Tyr Gly
35 180 185 190

Pro Ser Ala Thr Ser Glu Lys Cys Pro Gly Asn Ala Leu Glu Lys Gly
195 200 205

Gly Lys Gly Ser Ile Thr Glu Gln Leu Leu Asn Ala Arg Ala Asp Val
40 210 215 220

Thr Leu Gly Gly Gly Ala Lys Thr Phe Ala Glu Thr Ala Thr Ala Gly
45 225 230 235 240

Glu Trp Gln Gly Lys Thr Leu Arg Glu Gln Ala Gln Ala Arg Gly Tyr
245 250 255

Gln Leu Val Ser Asp Ala Ala Ser Leu Asn Ser Val Thr Glu Ala Asn
50 260 265 270

Gln Gln Lys Pro Leu Leu Gly Leu Phe Ala Asp Gly Asn Met Pro Val

55

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	275		280		285	
5	Arg Trp Leu Gly Pro Lys Ala Thr Tyr His Gly Asn Ile Asp Lys Pro 290 295 300					
	Ala Val Thr Cys Thr Pro Asn Pro Gln Arg Asn Asp Ser Val Pro Thr 305 310 315 320					
10	Leu Ala Gln Met Thr Asp Lys Ala Ile Glu Leu Leu Ser Lys Asn Glu 325 330 335					
	Lys Gly Phe Phe Leu Gln Val Glu Gly Ala Ser Ile Asp Lys Gln Asp 340 345 350					
15	His Ala Ala Asn Pro Cys Gly Gln Ile Gly Glu Thr Val Asp Leu Asp 355 360 365					
	Glu Ala Val Gln Arg Ala Leu Glu Phe Ala Lys Lys Glu Gly Asn Thr 370 375 380					
20	Leu Val Ile Val Thr Ala Asp His Ala His Ala Ser Gln Ile Val Ala 385 390 395 400					
	Pro Asp Thr Lys Ala Pro Gly Leu Thr Gln Ala Leu Asn Thr Lys Asp 405 410 415					
	Gly Ala Val Met Val Met Ser Tyr Gly Asn Ser Glu Glu Asp Ser Gln 420 425 430					
30	Glu His Thr Gly Ser Gln Leu Arg Ile Ala Ala Tyr Gly Pro His Ala 435 440 445					
	Ala Asn Val Val Gly Leu Thr Asp Gln Thr Asp Leu Phe Tyr Thr Met 450 455 460					
35	Lys Ala Ala Leu Gly Leu Lys 465 470					
40	<210> 9 <211> 1024 <212> PRT <213> Escherichia coli					
45	<400> 9					
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50	Trp Glu Asn Pro Gly Val Thr Gln Leu Asn Arg Leu Ala Ala His Pro 20 25 30					
	Pro Phe Ala Ser Trp Arg Asn Ser Glu Glu Ala Arg Thr Asp Arg Pro 35 40 45					
55	Ser Gln Gln Leu Arg Ser Leu Asn Gly Glu Trp Arg Phe Ala Trp Phe 50 55 60					

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5 Pro Ala Pro Glu Ala Val Pro Glu Ser Trp Leu Glu Cys Asp Leu Pro
 65 70 75 80
 Glu Ala Asp Thr Val Val Val Pro Ser Asn Trp Gln Met His Gly Tyr
 85 90 95
 Asp Ala Pro Ile Tyr Thr Asn Val Thr Tyr Pro Ile Thr Val Asn Pro
 100 105 110
 10 Pro Phe Val Pro Thr Glu Asn Pro Thr Gly Cys Tyr Ser Leu Thr Phe
 115 120 125
 Asn Val Asp Glu Ser Trp Leu Gln Glu Gly Gln Thr Arg Ile Ile Phe
 130 135 140
 15 Asp Gly Val Asn Ser Ala Phe His Leu Trp Cys Asn Gly Arg Trp Val
 145 150 155 160
 20 Gly Tyr Gly Gln Asp Ser Arg Leu Pro Ser Glu Phe Asp Leu Ser Ala
 165 170 175
 Phe Leu Arg Ala Gly Glu Asn Arg Leu Ala Val Met Val Leu Arg Trp
 180 185 190
 25 Ser Asp Gly Ser Tyr Leu Glu Asp Gln Asp Met Trp Arg Met Ser Gly
 195 200 205
 Ile Phe Arg Asp Val Ser Leu Leu His Lys Pro Thr Thr Gln Ile Ser
 210 215 220
 30 Asp Phe His Val Ala Thr Arg Phe Asn Asp Asp Phe Ser Arg Ala Val
 225 230 235 240
 35 Leu Glu Ala Glu Val Gln Met Cys Gly Glu Leu Arg Asp Tyr Leu Arg
 245 250 255
 Val Thr Val Ser Leu Trp Gln Gly Glu Thr Gln Val Ala Ser Gly Thr
 260 265 270
 40 Ala Pro Phe Gly Gly Glu Ile Ile Asp Glu Arg Gly Gly Tyr Ala Asp
 275 280 285
 Arg Val Thr Leu Arg Leu Asn Val Glu Asn Pro Lys Leu Trp Ser Ala
 290 295 300
 45 Glu Ile Pro Asn Leu Tyr Arg Ala Val Val Glu Leu His Thr Ala Asp
 305 310 315 320
 50 Gly Thr Leu Ile Glu Ala Glu Ala Cys Asp Val Gly Phe Arg Glu Val
 325 330 335
 Arg Ile Glu Asn Gly Leu Leu Leu Leu Asn Gly Lys Pro Leu Leu Ile
 340 345 350
 55

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Arg Gly Val Asn Arg His Glu His His Pro Leu His Gly Gln Val Met
 355 360 365

5 Asp Glu Gln Thr Met Val Gln Asp Ile Leu Leu Met Lys Gln Asn Asn
 370 375 380

Phe Asn Ala Val Arg Cys Ser His Tyr Pro Asn His Pro Leu Trp Tyr
 385 390 395 400

10 Thr Leu Cys Asp Arg Tyr Gly Leu Tyr Val Val Asp Glu Ala Asn Ile
 405 410 415

Glu Thr His Gly Met Val Pro Met Asn Arg Leu Thr Asp Asp Pro Arg
 420 425 430

15 Trp Leu Pro Ala Met Ser Glu Arg Val Thr Arg Met Val Gln Arg Asp
 435 440 445

20 Arg Asn His Pro Ser Val Ile Ile Trp Ser Leu Gly Asn Glu Ser Gly
 450 455 460

His Gly Ala Asn His Asp Ala Leu Tyr Arg Trp Ile Lys Ser Val Asp
 465 470 475 480

25 Pro Ser Arg Pro Val Gln Tyr Glu Gly Gly Ala Asp Thr Thr Ala
 485 490 495

Thr Asp Ile Ile Cys Pro Met Tyr Ala Arg Val Asp Glu Asp Gln Pro
 500 505 510

30 Phe Pro Ala Val Pro Lys Trp Ser Ile Lys Lys Trp Leu Ser Leu Pro
 515 520 525

Gly Glu Thr Arg Pro Leu Ile Leu Cys Glu Tyr Ala His Ala Met Gly
 530 535 540

35 Asn Ser Leu Gly Gly Phe Ala Lys Tyr Trp Gln Ala Phe Arg Gln Tyr
 545 550 555 560

40 Pro Arg Leu Gln Gly Gly Phe Val Trp Asp Trp Val Asp Gln Ser Leu
 565 570 575

Ile Lys Tyr Asp Glu Asn Gly Asn Pro Trp Ser Ala Tyr Gly Gly Asp
 580 585 590

45 Phe Gly Asp Thr Pro Asn Asp Arg Gln Phe Cys Met Asn Gly Leu Val
 595 600 605

50 Phe Ala Asp Arg Thr Pro His Pro Ala Leu Thr Glu Ala Lys His Gln
 610 615 620

Gln Gln Phe Phe Gln Phe Arg Leu Ser Gly Gln Thr Ile Glu Val Thr
 625 630 635 640

55 Ser Glu Tyr Leu Phe Arg His Ser Asp Asn Glu Leu Leu His Trp Met

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				645					650				655			
5	Val	Ala	Leu	Asp	Gly	Lys	Pro	Leu	Ala	Ser	Gly	Glu	Val	Pro	Leu	Asp
				660					665					670		
	Val	Ala	Pro	Gln	Gly	Lys	Gln	Leu	Ile	Glu	Leu	Pro	Glu	Leu	Pro	Gln
			675					680					685			
10	Pro	Glu	Ser	Ala	Gly	Gln	Leu	Trp	Leu	Thr	Val	Arg	Val	Val	Gln	Pro
		690					695					700				
	Asn	Ala	Thr	Ala	Trp	Ser	Glu	Ala	Gly	His	Ile	Ser	Ala	Trp	Gln	Gln
	705					710					715					720
15	Trp	Arg	Leu	Ala	Glu	Asn	Leu	Ser	Val	Thr	Leu	Pro	Ala	Ala	Ser	His
				725						730					735	
	Ala	Ile	Pro	His	Leu	Thr	Thr	Ser	Glu	Met	Asp	Phe	Cys	Ile	Glu	Leu
20				740					745					750		
	Gly	Asn	Lys	Arg	Trp	Gln	Phe	Asn	Arg	Gln	Ser	Gly	Phe	Leu	Ser	Gln
			755					760					765			
25	Met	Trp	Ile	Gly	Asp	Lys	Lys	Gln	Leu	Leu	Thr	Pro	Leu	Arg	Asp	Gln
		770					775					780				
	Phe	Thr	Arg	Ala	Pro	Leu	Asp	Asn	Asp	Ile	Gly	Val	Ser	Glu	Ala	Thr
	785					790					795					800
30	Arg	Ile	Asp	Pro	Asn	Ala	Trp	Val	Glu	Arg	Trp	Lys	Ala	Ala	Gly	His
					805					810					815	
	Tyr	Gln	Ala	Glu	Ala	Ala	Leu	Leu	Gln	Cys	Thr	Ala	Asp	Thr	Leu	Ala
35				820					825					830		
	Asp	Ala	Val	Leu	Ile	Thr	Thr	Ala	His	Ala	Trp	Gln	His	Gln	Gly	Lys
			835					840					845			
40	Thr	Leu	Phe	Ile	Ser	Arg	Lys	Thr	Tyr	Arg	Ile	Asp	Gly	Ser	Gly	Gln
		850					855					860				
	Met	Ala	Ile	Thr	Val	Asp	Val	Glu	Val	Ala	Ser	Asp	Thr	Pro	His	Pro
45						870					875					880
	Ala	Arg	Ile	Gly	Leu	Asn	Cys	Gln	Leu	Ala	Gln	Val	Ala	Glu	Arg	Val
				885						890					895	
	Asn	Trp	Leu	Gly	Leu	Gly	Pro	Gln	Glu	Asn	Tyr	Pro	Asp	Arg	Leu	Thr
50				900					905					910		
	Ala	Ala	Cys	Phe	Asp	Arg	Trp	Asp	Leu	Pro	Leu	Ser	Asp	Met	Tyr	Thr
			915					920					925			
55	Pro	Tyr	Val	Phe	Pro	Ser	Glu	Asn	Gly	Leu	Arg	Cys	Gly	Thr	Arg	Glu
		930					935						940			

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Leu Asn Tyr Gly Pro His Gln Trp Arg Gly Asp Phe Gln Phe Asn Ile
945 950 955 960

5 Ser Arg Tyr Ser Gln Gln Gln Leu Met Glu Thr Ser His Arg His Leu
965 970 975

Leu His Ala Glu Glu Gly Thr Trp Leu Asn Ile Asp Gly Phe His Met
980 985 990

10 Gly Ile Gly Gly Asp Asp Ser Trp Ser Pro Ser Val Ser Ala Glu Phe
995 1000 1005

15 Gln Leu Ser Ala Gly Arg Tyr His Tyr Gln Leu Val Trp Cys Gln
1010 1015 1020

Lys

20 Claims

1. A method of depleting a molecule from a solution, comprising contacting the solution with a microtube which comprises an electrospun shell, an electrospun coat over an internal surface of said shell and a member of an affinity pair attached to said microtube, wherein said member of said affinity pair is selected capable of binding the molecule, thereby depleting the molecule from the solution.
2. The method of claim 1, further comprising collecting said solution following said contacting.
3. The method of claim 2, wherein said solution comprises blood.
4. A method of isolating a molecule from a solution, comprising:
 - (a) contacting the solution with a microtube which comprises an electrospun shell, an electrospun coat over an internal surface of said shell and a member of an affinity pair attached to said microtube under conditions which allow binding of the molecule to the microtube via said member of said affinity pair which is selected capable of binding the molecule, and;
 - (b) eluting the molecule from the microtube;thereby isolating the molecule from the solution.
5. The method of claim 1, 2, 3, or 4, wherein said affinity pair is selected from the group consisting of an enzyme and a substrate, a hormone and a receptor, an antibody and an antigen, a polypeptide and a polynucleotide, a polynucleotide and a cognate polynucleotide, a polypeptide and a metal ion, a polypeptide and a carbohydrate.
6. The method of any of claims 1-5, wherein said shell comprises a polymer selected from the group consisting of poly(e-caprolactone) (PCL), polyamide, poly(siloxane), poly(silicone), poly(ethylene), poly(vinyl pyrrolidone), poly(2-hydroxy ethylmethacrylate), poly(N-vinyl pyrrolidone), poly(methyl methacrylate), poly(vinyl alcohol), poly(acrylic acid), poly(vinyl acetate), polyacrylamide, poly(ethylene-co-vinyl acetate), poly(ethylene glycol), poly(methacrylic acid), polylactide, polyglycolide, poly(lactide-coglycolide), polyanhydride, polyorthoester, poly(carbonate), poly(acrylonitrile), poly(ethylene oxide), polyaniline, polyvinyl carbazole, polystyrene, poly(vinyl phenol), polyhydroxyacid, poly(caprolactone), polyanhydride, polyhydroxyalkanoate, polyurethane, collagen, albumin, alginate, chitosan, starch, hyaluronic acid, and whereas said electrospun coat comprises a polymer selected from the group consisting of poly(acrylic acid), poly(vinyl acetate), polyacrylamide, poly(ethylene-co-vinyl acetate), poly(ethylene glycol), poly(methacrylic acid), polylactide polyglycolide, poly(lactide-coglycolide), polyanhydride, polyorthoester, poly(carbonate), poly(ethylene oxide), polyaniline, polyvinyl carbazole, polystyrene, poly(vinyl phenol), polyhydroxyacid, alginate, starch, hyaluronic acid.
7. The method of any of claims 1-6, wherein a thickness of said shell is from about 100 nm to about 20 micrometer.

8. The method of any of claims 1-7, wherein an internal diameter of the microtube is from about 50 nm to about 20 micrometer.
9. The method of any of claims 1-8, wherein said member of said affinity pair is attached to said coat over said internal surface of said shell.
10. The method of any of claims 1-8, wherein said member of said affinity pair is attached to said shell of the microtube.
11. The method of any of claims 1-10, wherein said shell comprises pores.

Patentansprüche

1. Verfahren zum Abreichern eines Moleküls aus einer Lösung, das das Inkontaktbringen der Lösung mit einem Mikroröhrchen umfasst, das eine elektrogessponnene Hülle, einen elektrogessponnenen Mantel über einer Innenfläche der Hülle und ein Element eines Affinitätspaars umfasst, das am Mikroröhrchen angebracht ist, wobei das Element des Affinitätspaars so ausgewählt ist, dass es zur Bindung des Moleküls in der Lage ist, wodurch das Molekül aus der Lösung abgereichert wird.
2. Verfahren nach Anspruch 1, das ferner das Sammeln der Lösung nach dem Inkontaktbringen umfasst.
3. Verfahren nach Anspruch 2, wobei die Lösung Blut umfasst.
4. Verfahren zum Isolieren eines Moleküls aus einer Lösung, das umfasst:
- (a) Inkontaktbringen der Lösung mit einem Mikroröhrchen, das eine elektrogessponnene Hülle, einen elektrogessponnenen Mantel über einer Innenfläche der Hülle und ein Element eines Affinitätspaars, das am Mikroröhrchen angebracht ist, unter Bedingungen umfasst, die das Binden des Moleküls an das Mikroröhrchen über das Element des Affinitätspaars ermöglichen, das so ausgewählt ist, dass es zur Bindung des Moleküls in der Lage ist; und
- (b) Eluieren des Moleküls aus dem Mikroröhrchen;
- wodurch das Molekül aus der Lösung isoliert wird.
5. Verfahren nach Anspruch 1, 2, 3 oder 4, wobei das Affinitätspaar aus der Gruppe ausgewählt ist, bestehend aus einem Enzym und einem Substrat, einem Hormon und einem Rezeptor, einem Antikörper und einem Antigen, einem Polypeptid und einem Polynukleotid, einem Polynukleotid und einem verwandten Polynukleotid, einem Polypeptid und einem Metallion, einem Polypeptid und einem Kohlenhydrat.
6. Verfahren nach einem der Ansprüche 1 bis 5, wobei die Hülle ein Polymer umfasst, das aus der Gruppe ausgewählt ist, bestehend aus Poly(ϵ -caprolacton) (PCL), Polyamid, Poly(siloxan), Poly(silikon), Poly(ethylen), Poly(vinylpyrrolidon), Poly(2-hydroxyethylmethacrylat), Poly(N-vinylpyrrolidon), Poly(methylmethacrylat), Poly(vinylalkohol), Poly(acrylsäure), Polyvinylacetat, Polyacrylamid, Poly(ethylen-co-vinylacetat), Poly(ethylenglycol), Poly(methacrylsäure), Polylactid, Polyglycolid, Poly(lactid-coglycolid), Polyanhydrid, Polyorthoester, Poly(carbonat), Poly(acrylonitril), Poly(ethylenoxid), Polyanilin, Polyvinylcarbazol, Polystyrol, Poly(vinylphenol), Polyhydroxysäure, Poly(caprolacton), Polyanhydrid, Polyhydroxyalkanoat, Polyurethan, Kollagen, Albumin, Alginate, Chitosan, Stärke, Hyaluronsäure, und wogegen der elektrogessponnene Mantel ein Polymer umfasst, das aus der Gruppe ausgewählt ist, bestehend aus Poly(acrylsäure), Poly(vinylacetat), Polyacrylamid, Poly(ethylen-co-vinylacetat), Poly(ethylenglycol), Poly(methacrylsäure), Polylactidpolyglycolid, Poly(lactid-coglycolid), Polyanhydrid, Polyorthoester, Poly(carbonat), Poly(ethylenoxid), Polyanilin, Polyvinylcarbazol, Polystyrol, Poly(vinylphenol), Polyhydroxysäure, Alginat, Stärke, Hyaluronsäure.
7. Verfahren nach einem der Ansprüche 1 bis 6, wobei eine Dicke der Hülle ungefähr 100 nm bis ungefähr 20 Mikrometer beträgt.
8. Verfahren nach einem der Ansprüche 1 bis 7, wobei ein Innendurchmesser des Mikroröhrchens ungefähr 50 nm bis ungefähr 20 Mikrometer beträgt.

9. Verfahren nach einem der Ansprüche 1 bis 8, wobei das Element des Affinitätspaars am Mantel über der Innenfläche der Hülle angebracht ist.
10. Verfahren nach einem der Ansprüche 1 bis 8, wobei das Element des Affinitätspaars an der Hülle des Mikroröhrchen angebracht ist.
11. Verfahren nach einem der Ansprüche 1 bis 10, wobei die Hülle Poren umfasst.

Revendications

1. Procédé pour éliminer une molécule d'une solution, comprenant la mise en contact de la solution avec un microtube qui comprend un corps électrofilé, un revêtement électrofilé sur une surface interne dudit corps et un membre d'une paire d'affinité attaché audit microtube, où ledit membre de ladite paire d'affinité est sélectionné pour être capable de se lier à la molécule, en éliminant ainsi la molécule de la solution.
2. Procédé selon la revendication 1, comprenant en outre la collecte de ladite solution après ladite mise en contact.
3. Procédé selon la revendication 2, dans lequel ladite solution comprend du sang.
4. Procédé pour isoler une molécule à partir d'une solution, comprenant :

- (a) la mise en contact de la solution avec un microtube qui comprend un corps électrofilé, un revêtement électrofilé sur une surface interne dudit corps et un membre d'une paire d'affinité attaché audit microtube dans des conditions qui permettent la liaison de la molécule au microtube via ledit membre de ladite paire d'affinité qui est sélectionné pour être capable de se lier à la molécule, et ;
- (b) l'élution de la molécule à partir du microtube ;

en isolant ainsi la molécule à partir de la solution.

5. Procédé selon la revendication 1, 2, 3 ou 4, dans lequel ladite paire d'affinité est sélectionnée dans le groupe consistant en une enzyme et un substrat, une hormone et un récepteur, un anticorps et un antigène, un polypeptide et un polynucléotide, un polynucléotide et un polynucléotide apparenté, un polypeptide et un ion métallique, un polypeptide et un glucide.
6. Procédé selon l'une quelconque des revendications 1-5, dans lequel ledit corps comprend un polymère sélectionné dans le groupe consistant en la poly(e-caprolactone) (PCL), le polyamide, le polysiloxane, le polysilicone, le polyéthylène, la polyvinylpyrrolidone, le poly(2-hydroxyéthylméthacrylate), la poly-N-vinylpyrrolidone, le polyméthacrylate de méthyle, l'alcool polyvinylique, le poly(acide acrylique), le polyacétate de vinyle, le polyacrylamide, le poly(éthylène-co-acétate de vinyle), le polyéthylène glycol, l'acide polyméthacrylique, le polylactide, le polyglycolide, le poly(lactide-co-glycolide), un polyanhydride, un polyorthoester, le polycarbonate, le polyacrylonitrile, l'oxyde de polyéthylène, la polyaniline, le polyvinylcarbazole, le polystyrène, le polyvinylphénol, un polyhydroxyacide, la polycaprolactone, un polyanhydride, un polyhydroxyalcanoate, le polyuréthane, le collagène, l'albumine, l'alginate, le chitosane, l'amidon, l'acide hyaluronique, alors que ledit revêtement électrofilé comprend un polymère sélectionné dans le groupe consistant en le poly(acide acrylique), l'acétate de polyvinyle, le polyacrylamide, le poly(éthylène-co-acétate de vinyle), le polyéthylène glycol, l'acide polyméthacrylique, le polylactide, le polyglycolide, le poly(lactide-co-glycolide), un polyanhydride, un polyorthoester, le polycarbonate, l'oxyde de polyéthylène, la polyaniline, le polyvinylcarbazole, le polystyrène, le polyvinylphénol, un polyhydroxyacide, l'alginate, l'amidon, l'acide hyaluronique.
7. Procédé selon l'une quelconque des revendications 1-6, dans lequel l'épaisseur dudit corps est comprise entre environ 100 nm et environ 20 micromètres.
8. Procédé selon l'une quelconque des revendications 1-7, dans lequel le diamètre interne du microtube est compris entre environ 50 nm et environ 20 micromètres.
9. Procédé selon l'une quelconque des revendications 1-8, dans lequel ledit membre de ladite paire d'affinité est attaché audit revêtement sur ladite surface interne dudit corps.

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10. Procédé selon l'une quelconque des revendications 1-8, dans lequel ledit membre de ladite paire d'affinité est attaché audit corps du microtubule.

11. Procédé selon l'une quelconque des revendications 1-10, dans lequel ledit corps comprend des pores.

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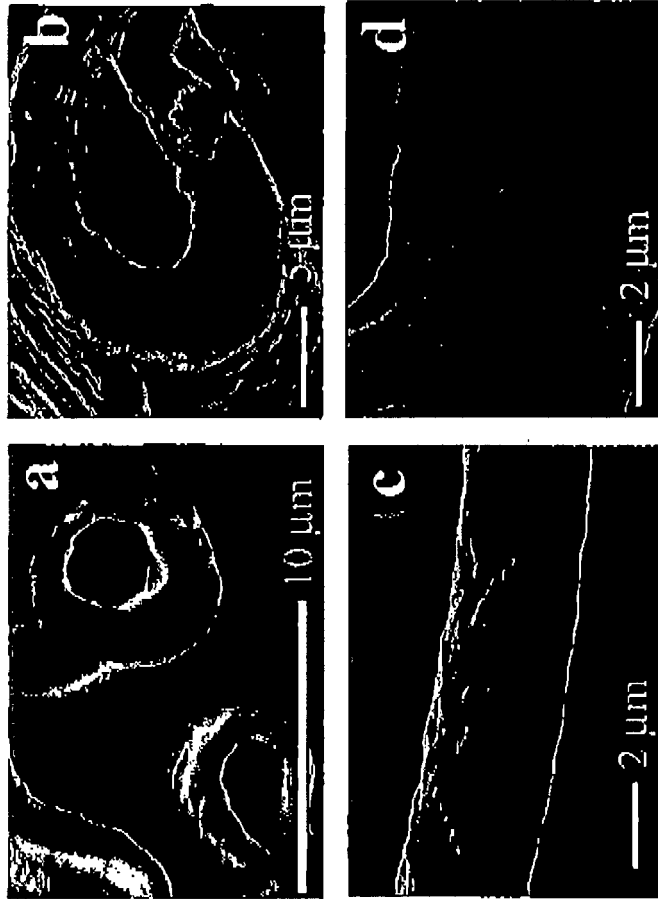
35

40

45

50

55



FIGS. 1A-D

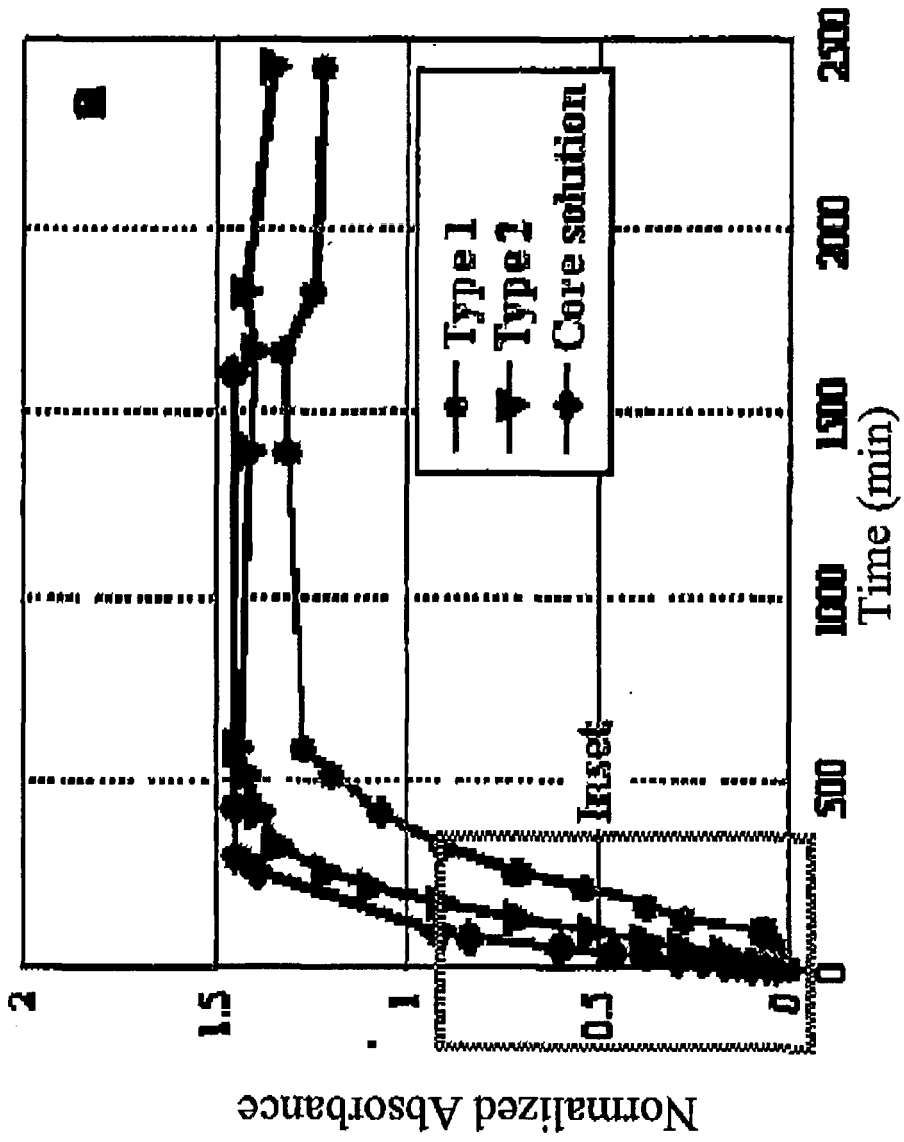


FIG. 2A

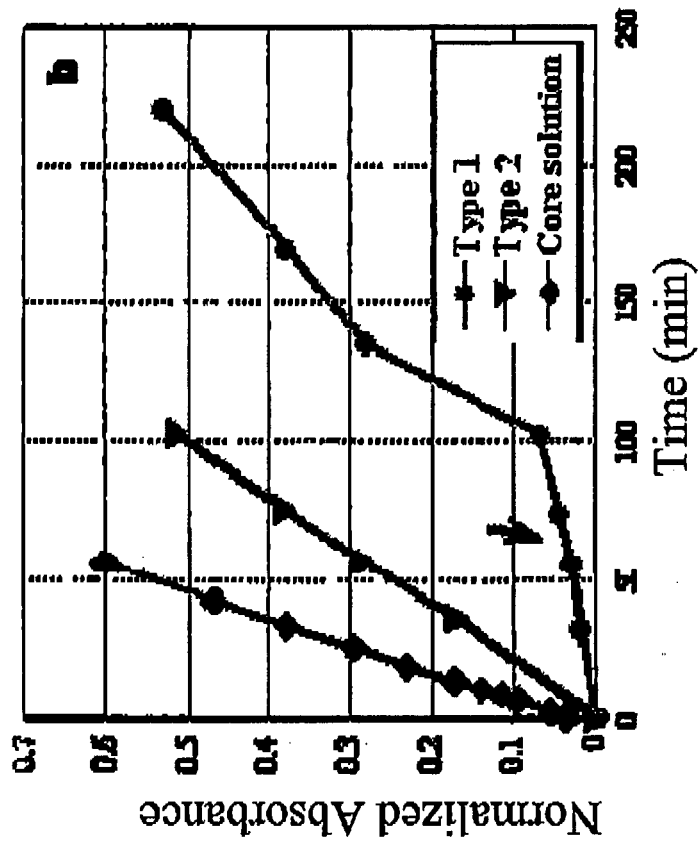


FIG. 2B

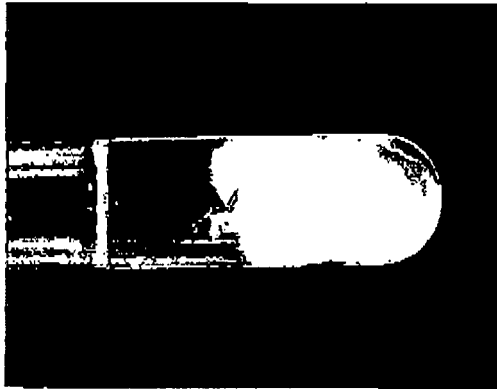


FIG. 2C

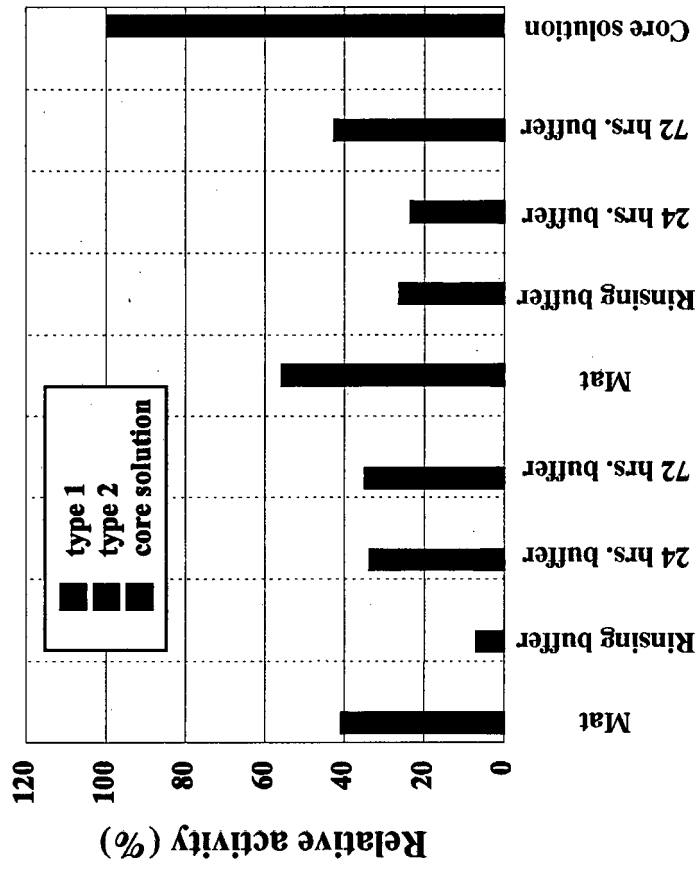


FIG. 3

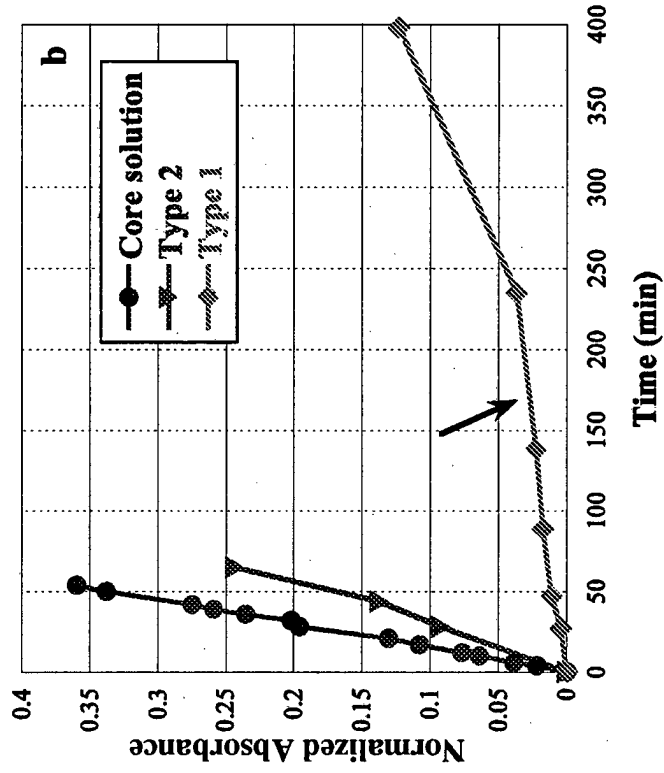


FIG. 4B

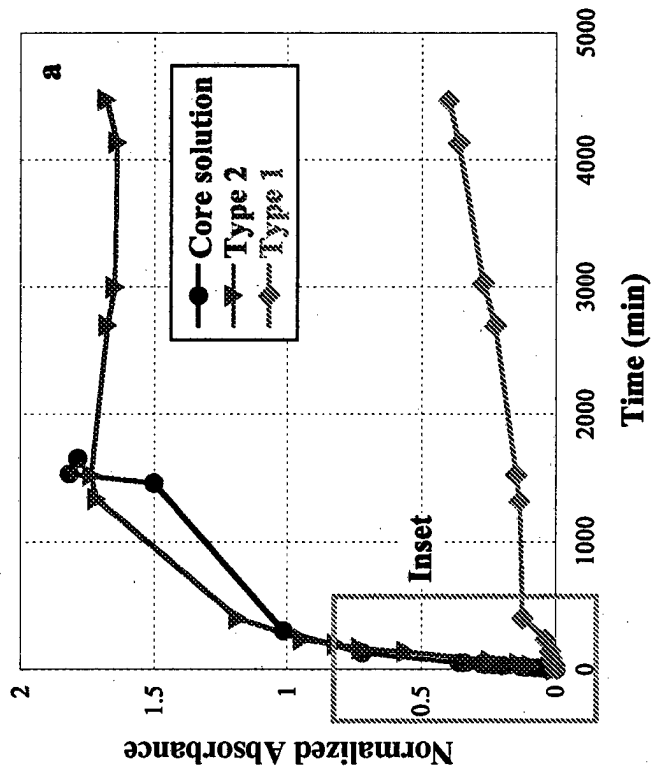


FIG. 4A

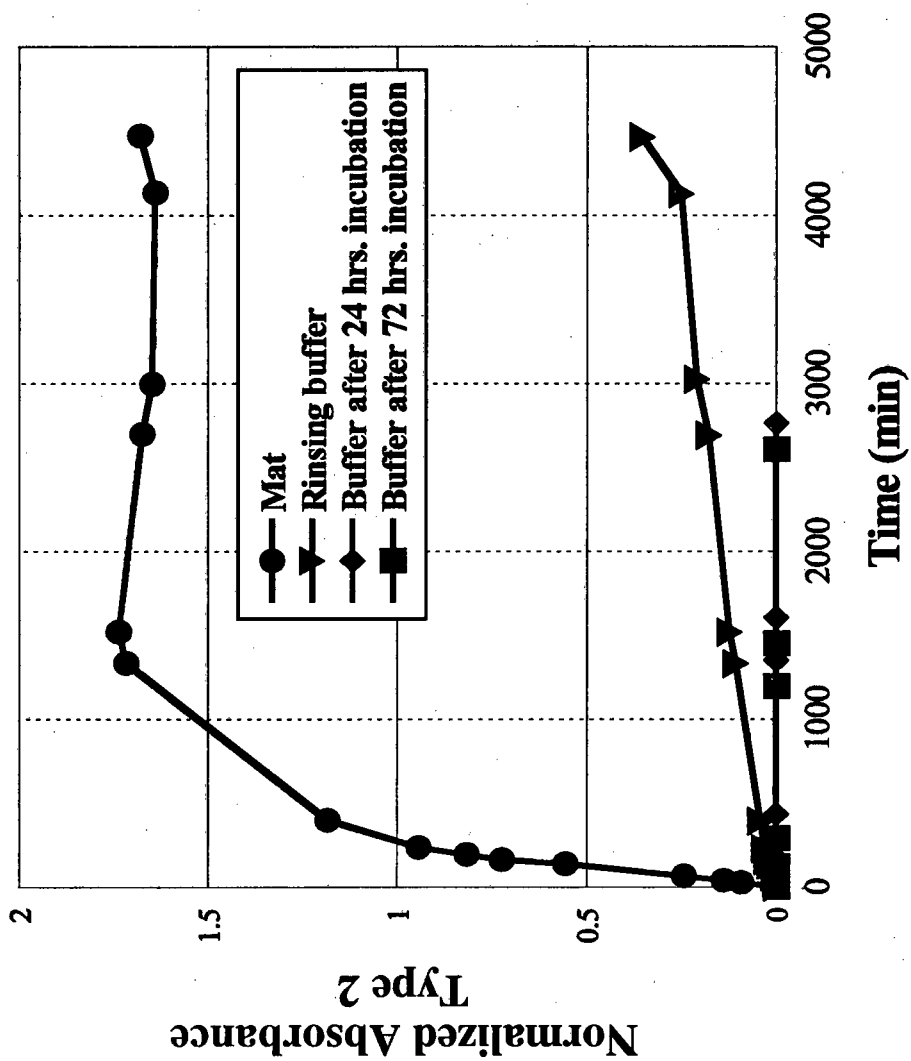


FIG. 5

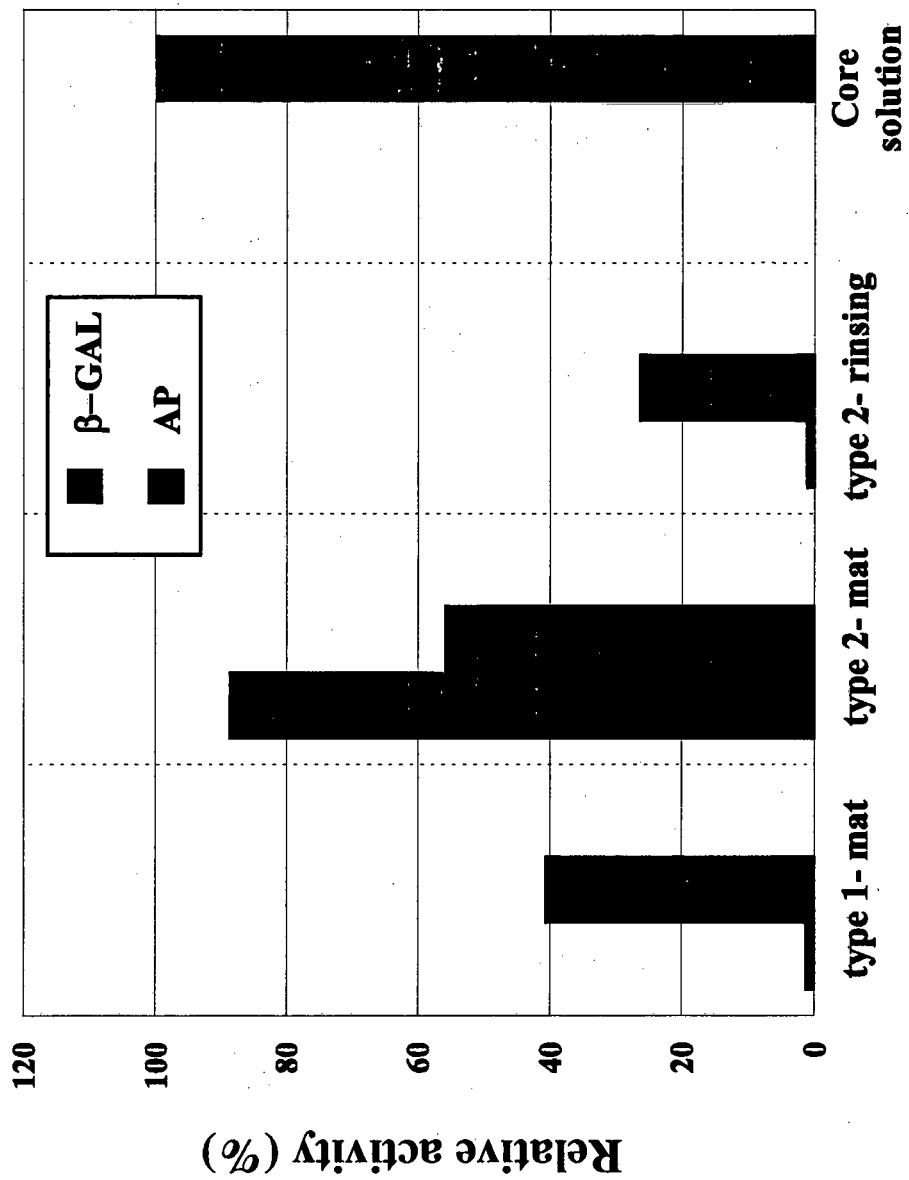
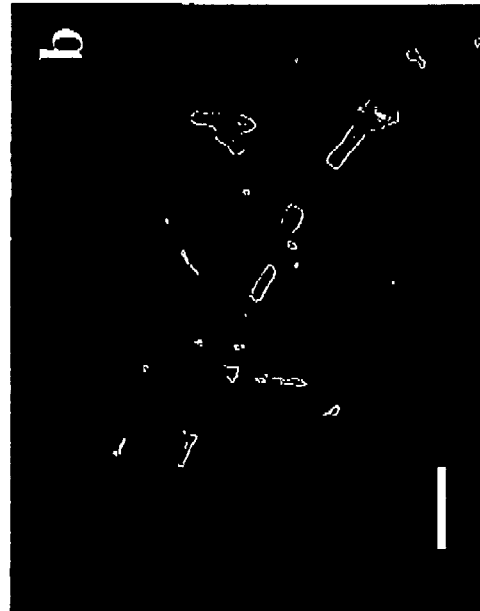


FIG. 6

FIG. 7A



FIG. 7B



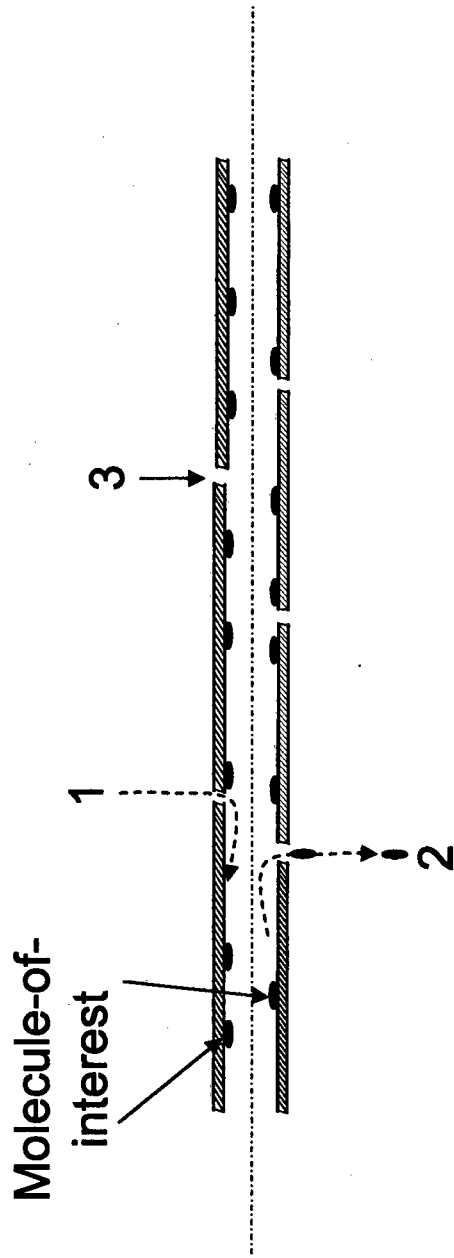


FIG. 8

Multiple Enzyme Pathways

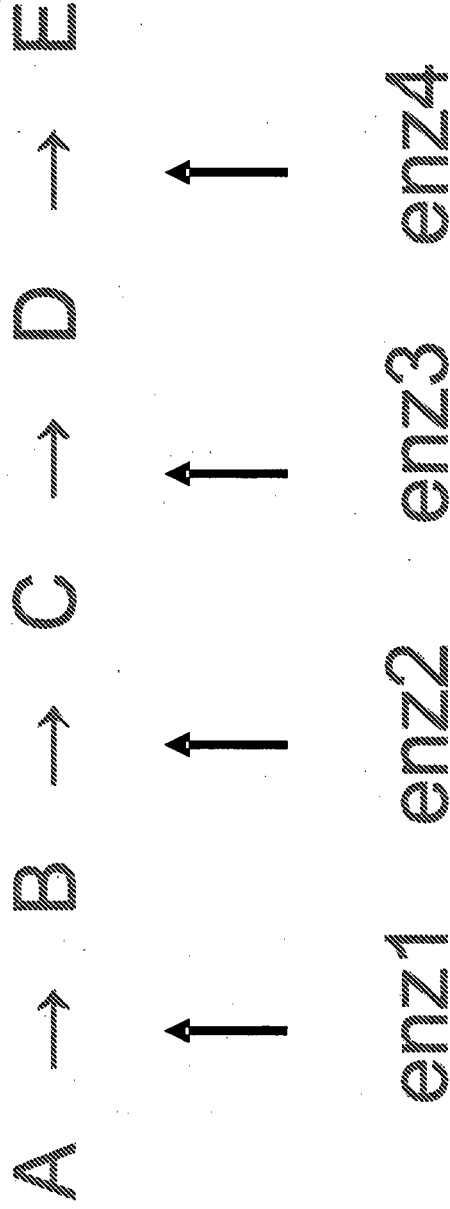
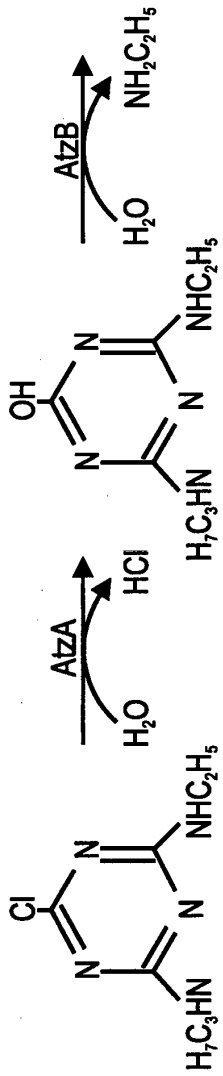
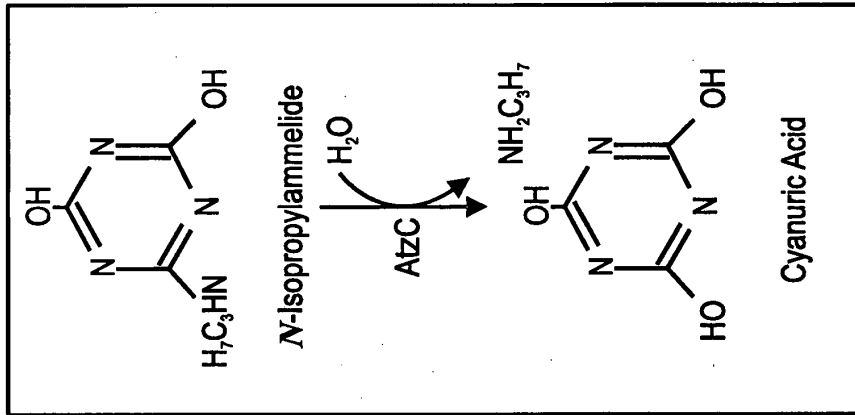
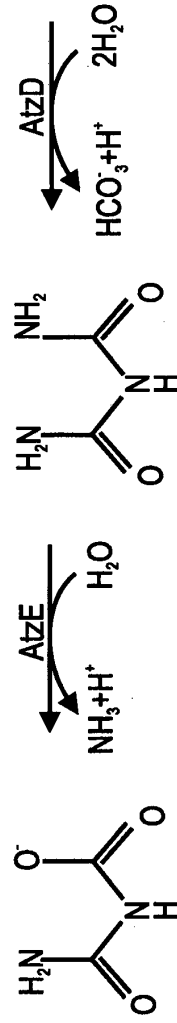


FIG. 9



Hydroxytriazine



Biuret



Allophanate

FIG. 10

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摘要(译)

本发明提供了一种通过同轴毛细管共同静电纺丝两种聚合物溶液将一种感兴趣的分子连接到微管上的方法，其中两种聚合物溶液的第一聚合物溶液用于形成微管的壳体，第二种聚合物溶液用于形成微管的壳体。两种聚合物溶液的聚合物溶液用于在壳的内表面上形成涂层，选择第一聚合物溶液比第二聚合物溶液更快固化，并且选择第二聚合物溶液的溶剂不能溶解第一聚合物溶液并且其中第二聚合物溶液包含感兴趣的分子，从而将感兴趣的分子附着到微管上。还提供了一种静电纺丝微管，其包含电纺壳，在壳的内表面上的电纺涂层和附着于微管的感兴趣的分子。

(1)

$$\text{Unit} = \frac{\Delta A}{\Delta t} \cdot 1000$$