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HANCOCK et al.(10) **Pub. No.: US 2019/0069951 A1**(43) **Pub. Date: Mar. 7, 2019**(54) **ELECTROSURGICAL PROBE FOR
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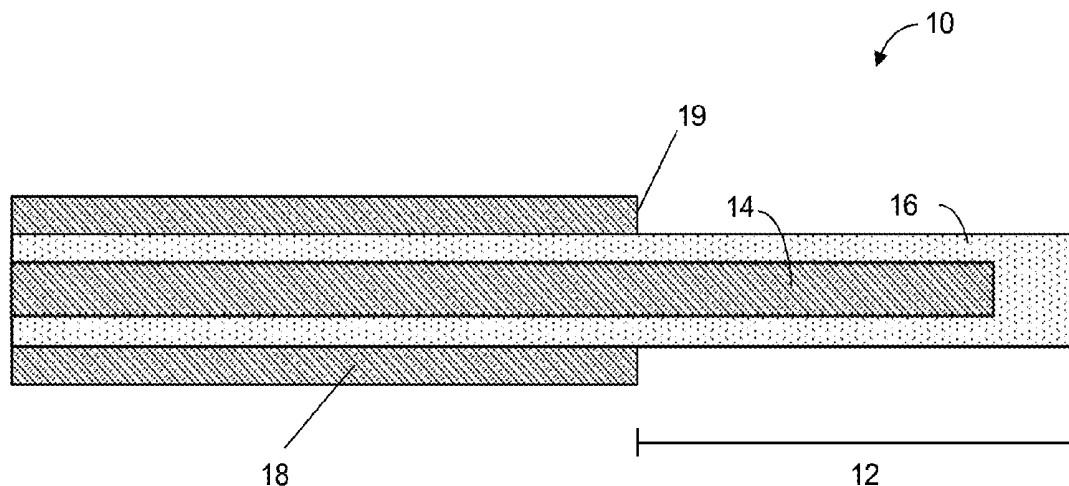
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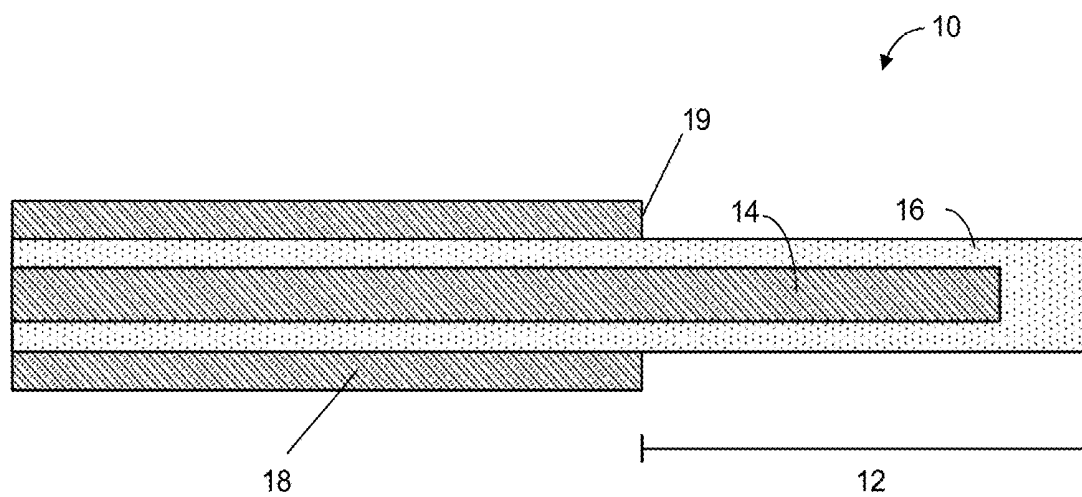
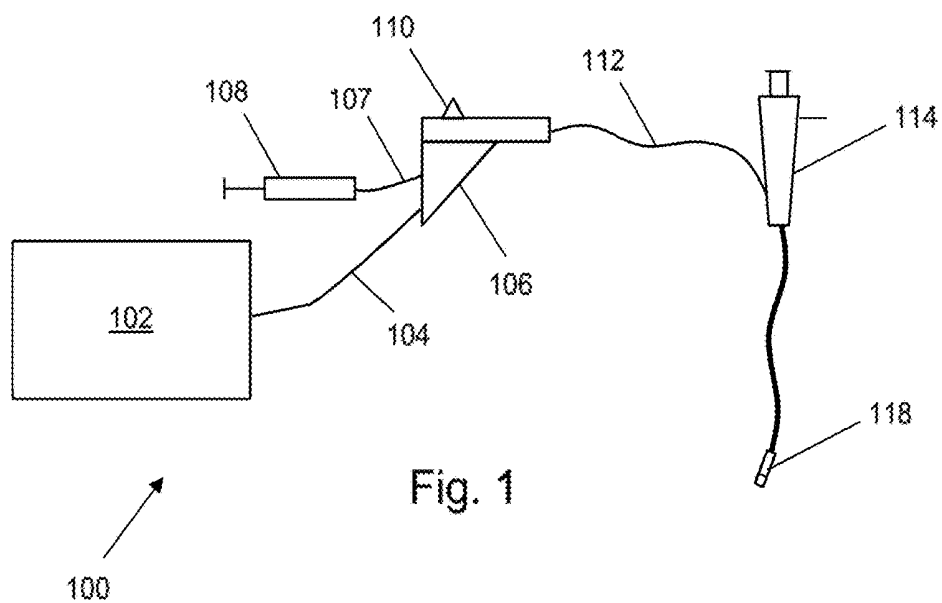
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(57)

ABSTRACT

An electrosurgical instrument for use in minimally invasive surgical techniques that provides a small scale localized microwave field capable of precisely ablating tissue, e.g. in the lungs, through suitable selection of geometry and material for a radiating distal tip thereof. The instrument may be used with a bronchoscope having a power delivery structure formed within the instrument cord thereof. A vision system may be incorporated into the energy delivery structure. The instrument comprise a coaxial cable for conveying microwave energy to a radiating tip portion that comprises a dielectric tip and a distal conductive portion that extends longitudinally therein. The dielectric tip has a dielectric constant greater than a dielectric material within the coaxial cable. The distal end of the device is designed to facilitate efficient microwave energy delivery into lung tumour tissue to achieve a localized volume of ablation.





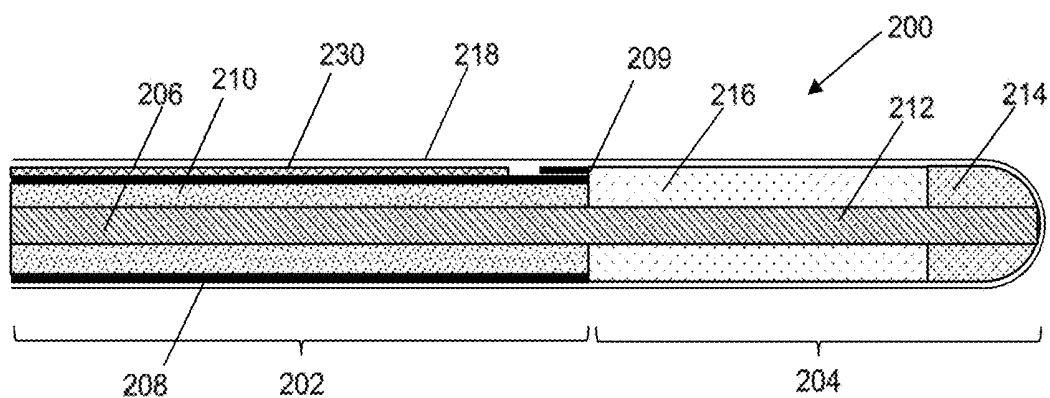


Fig. 3

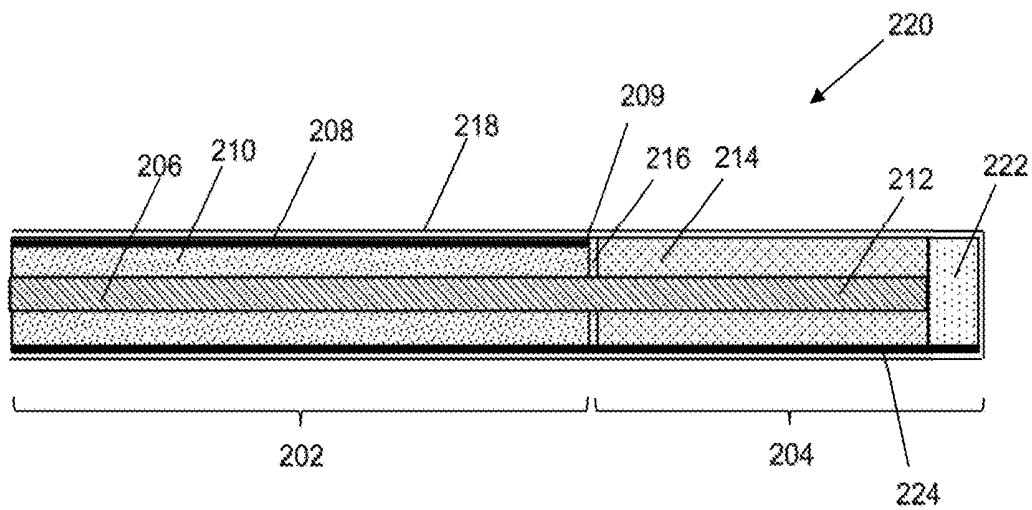


Fig. 4

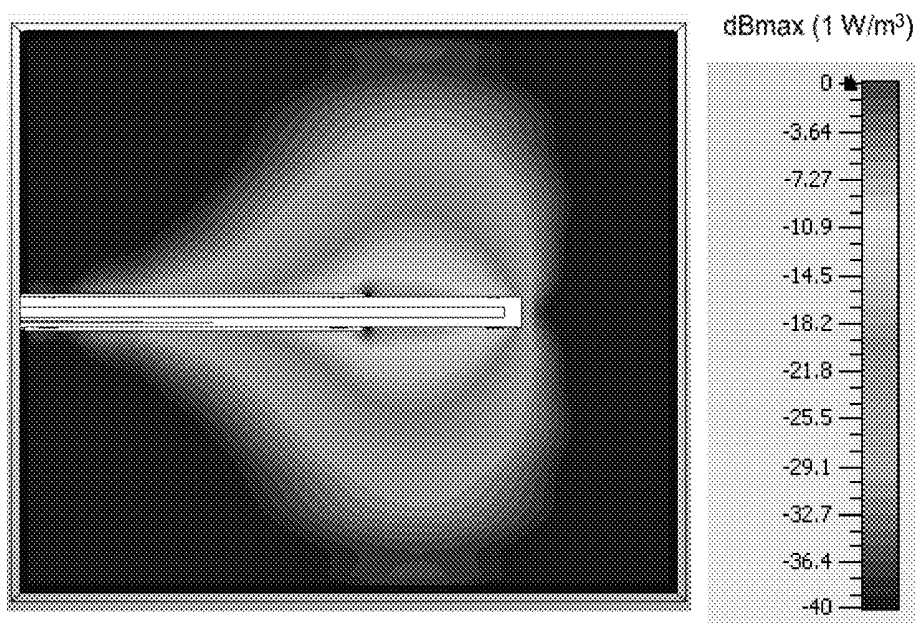


Fig. 5A

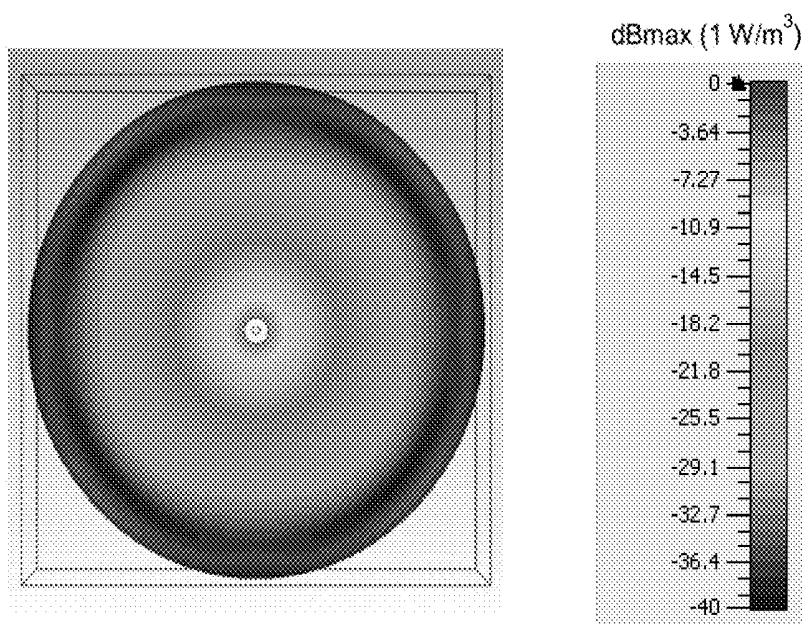


Fig. 5B

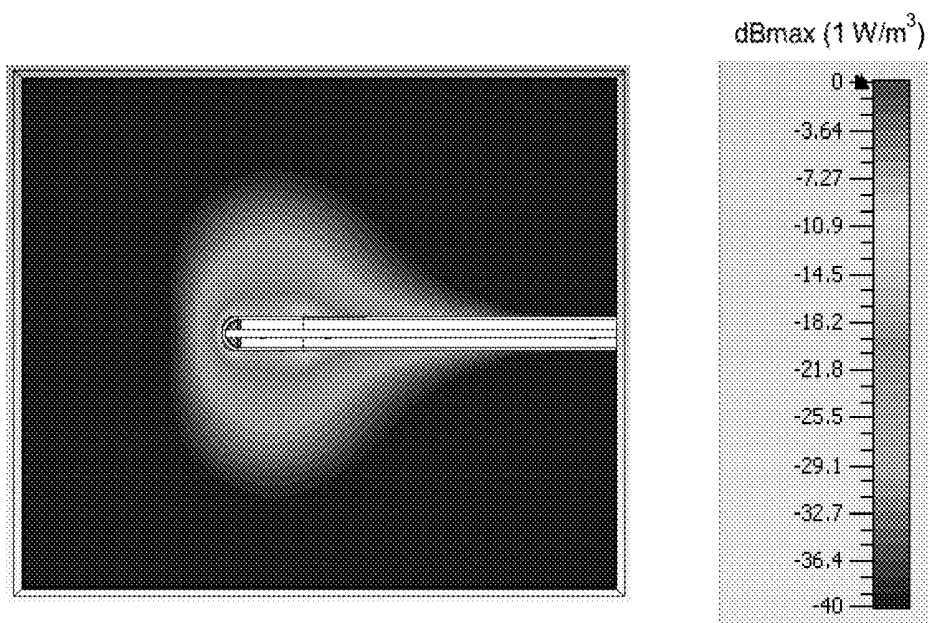


Fig. 6

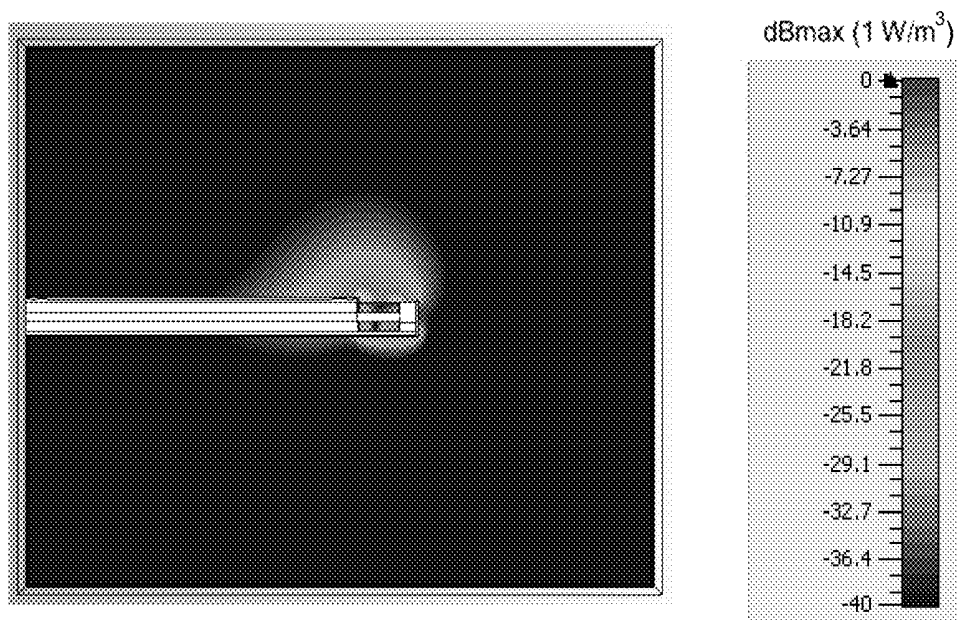


Fig. 7A

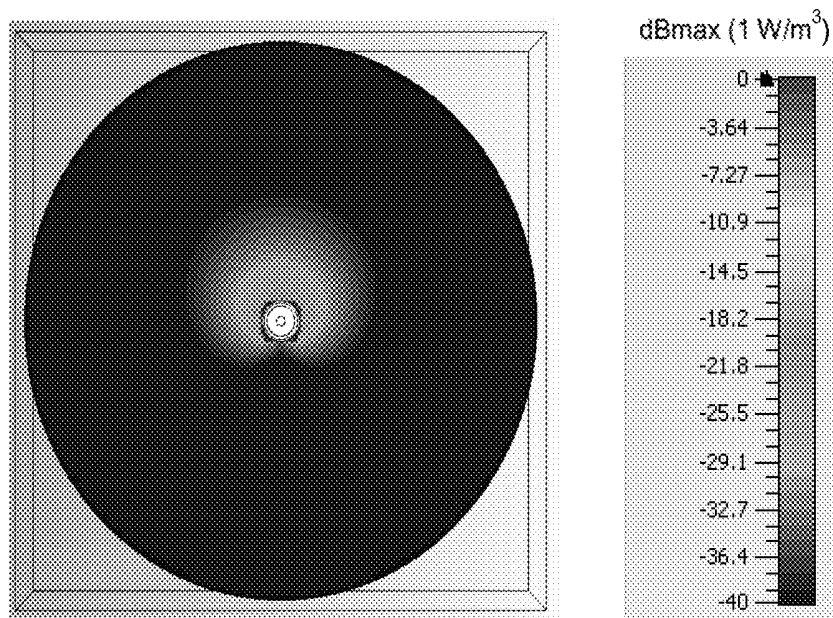


Fig. 7B

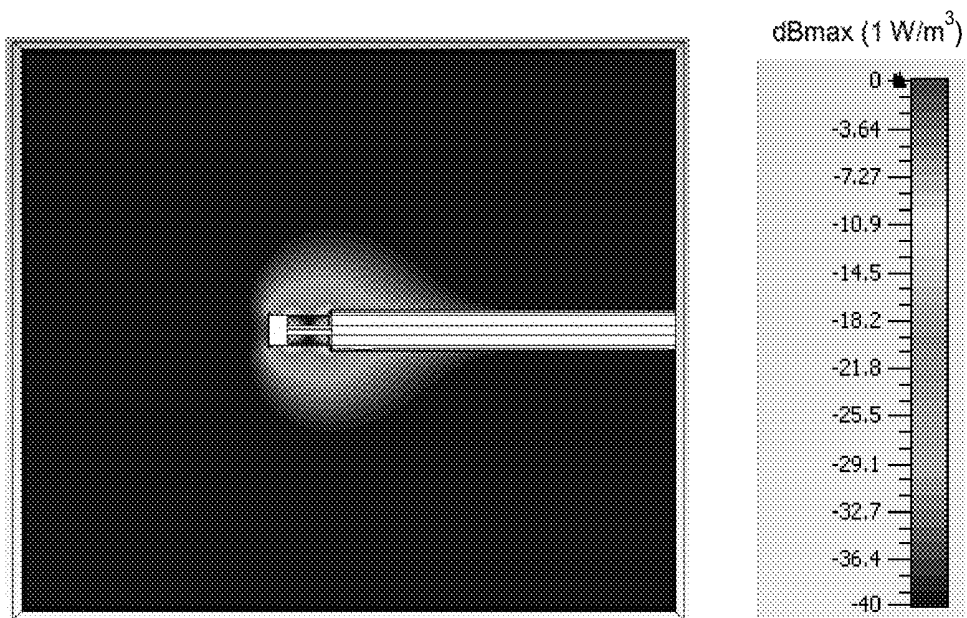


Fig. 7C

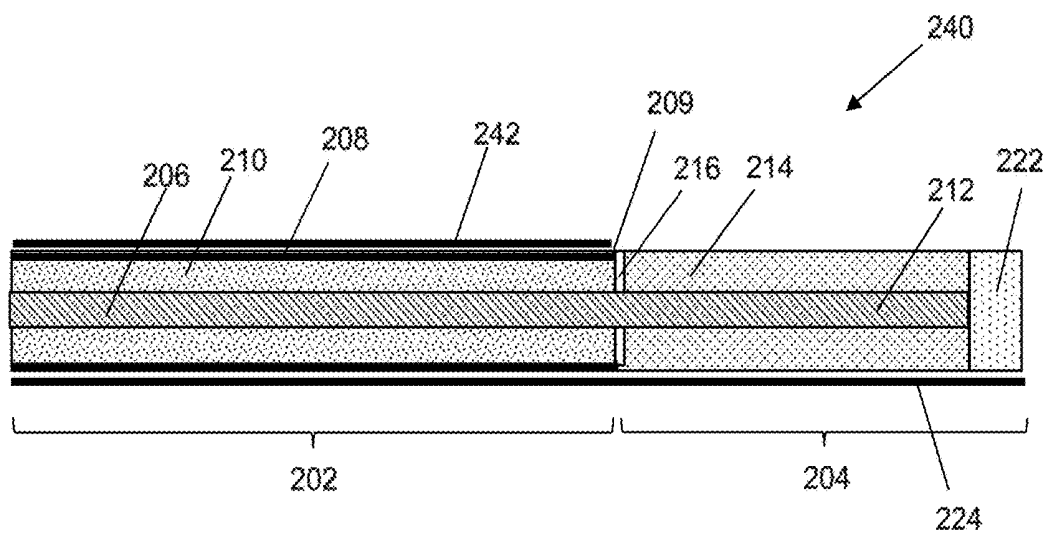


Fig. 8A

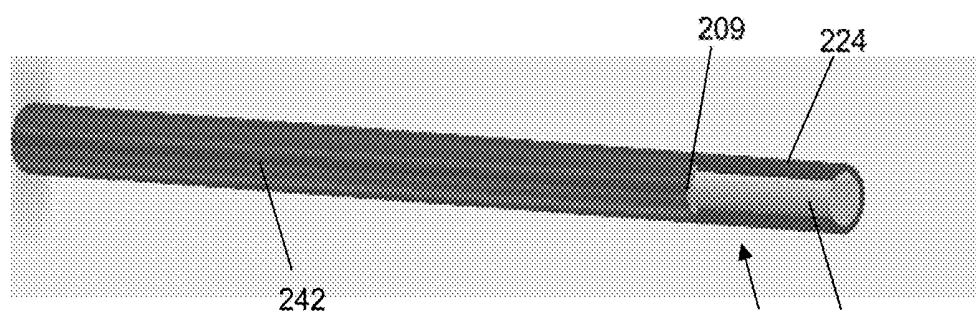


Fig. 8B

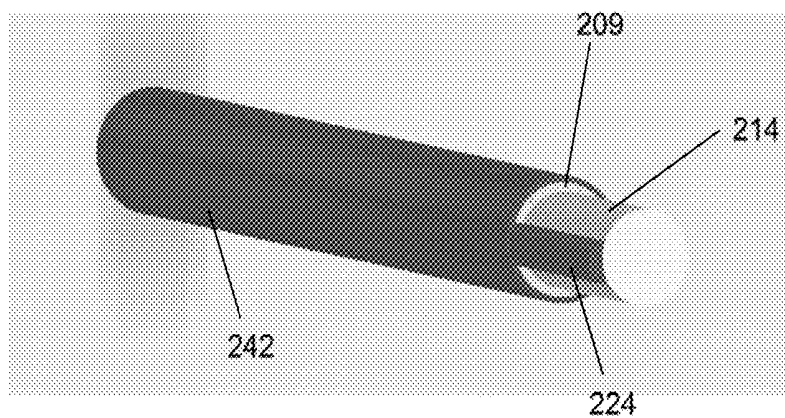


Fig. 8C

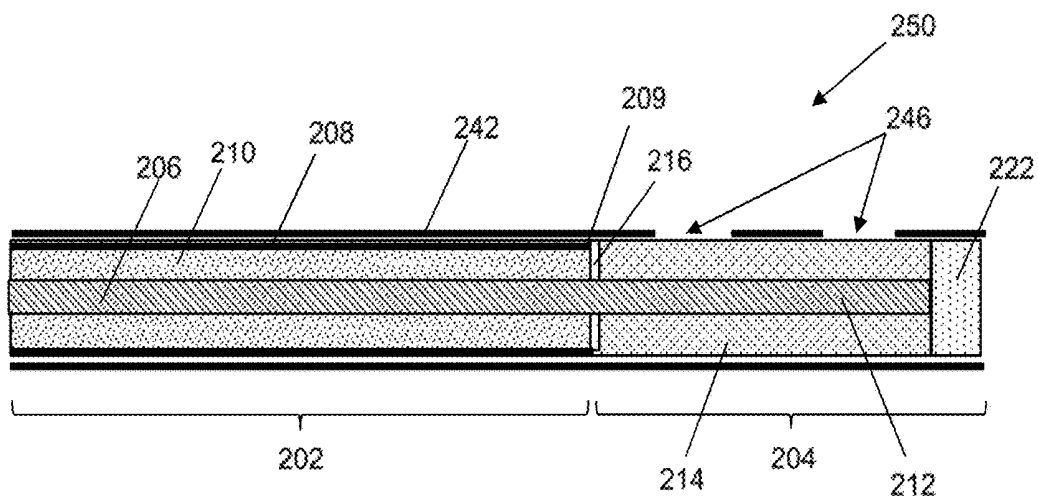


Fig. 9A

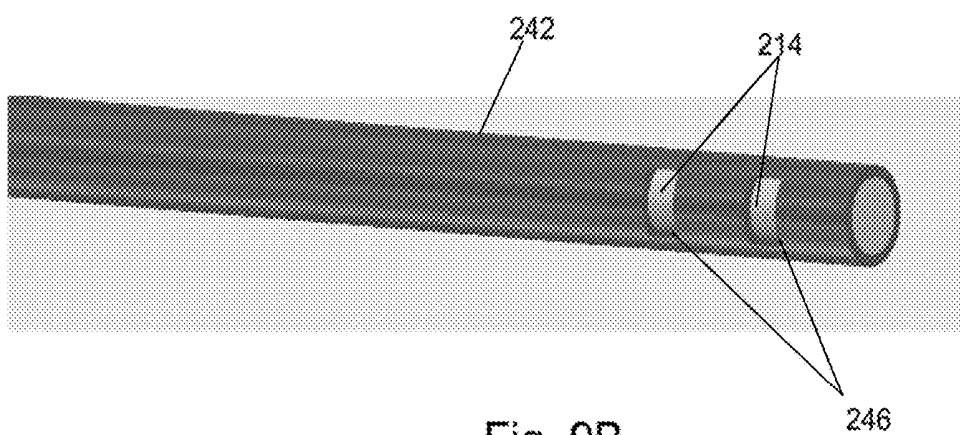


Fig. 9B

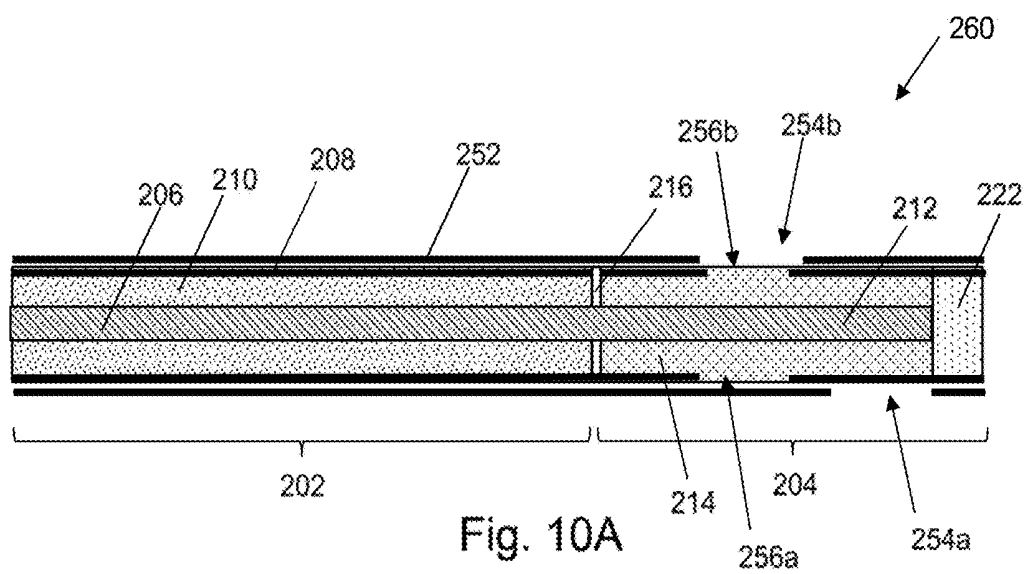


Fig. 10A

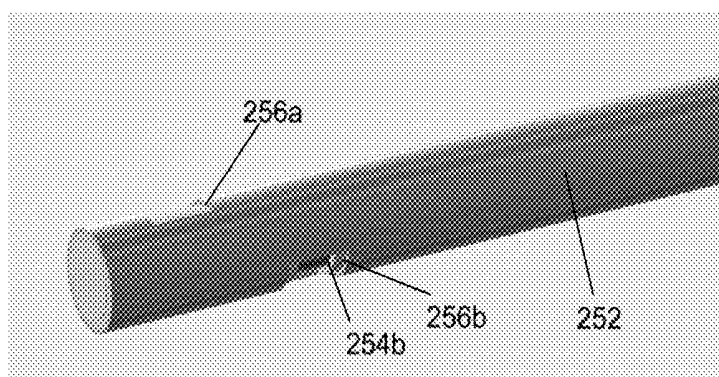


Fig. 10B

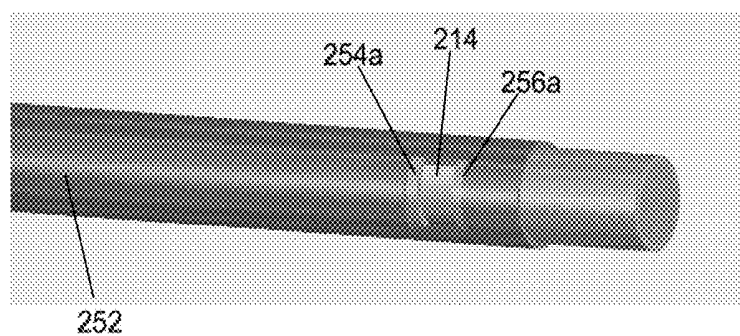


Fig. 10C

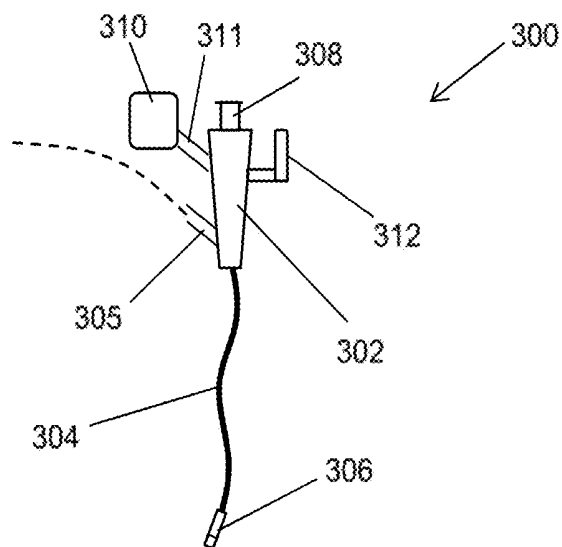


Fig. 11

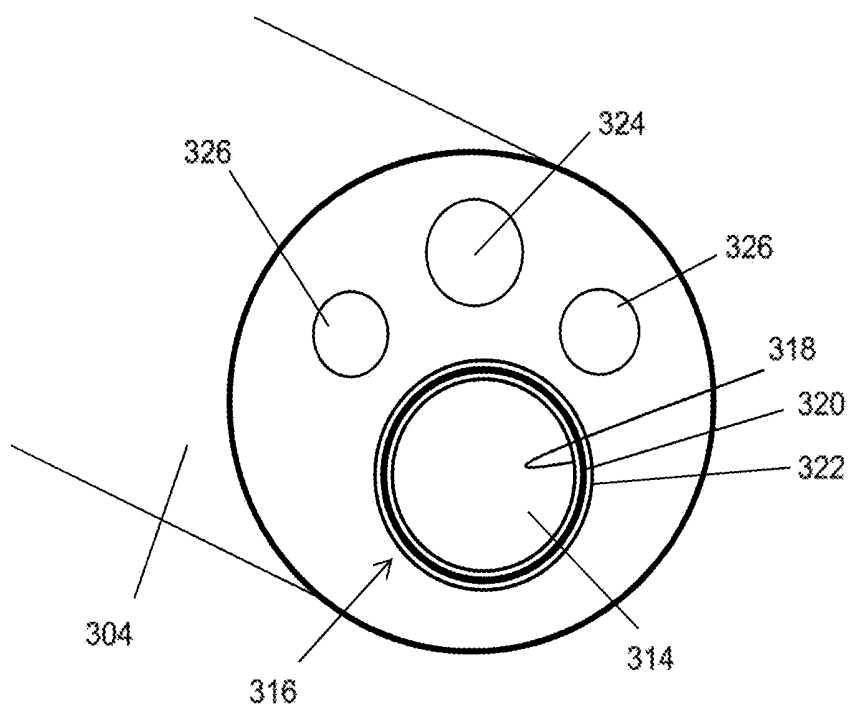
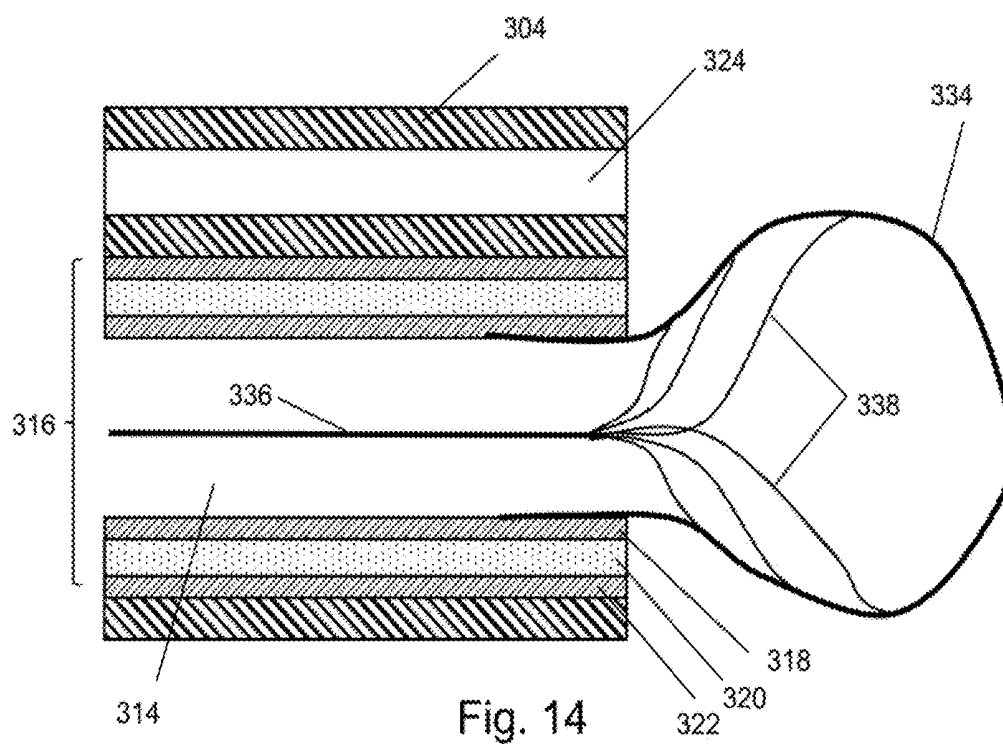
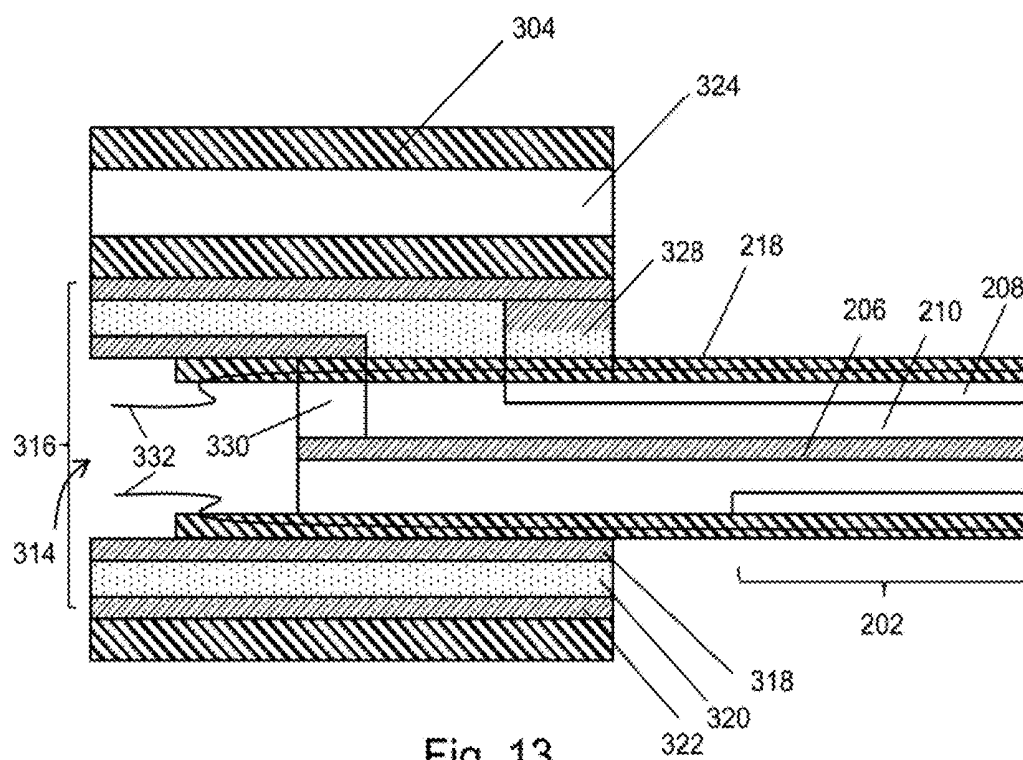


Fig. 12



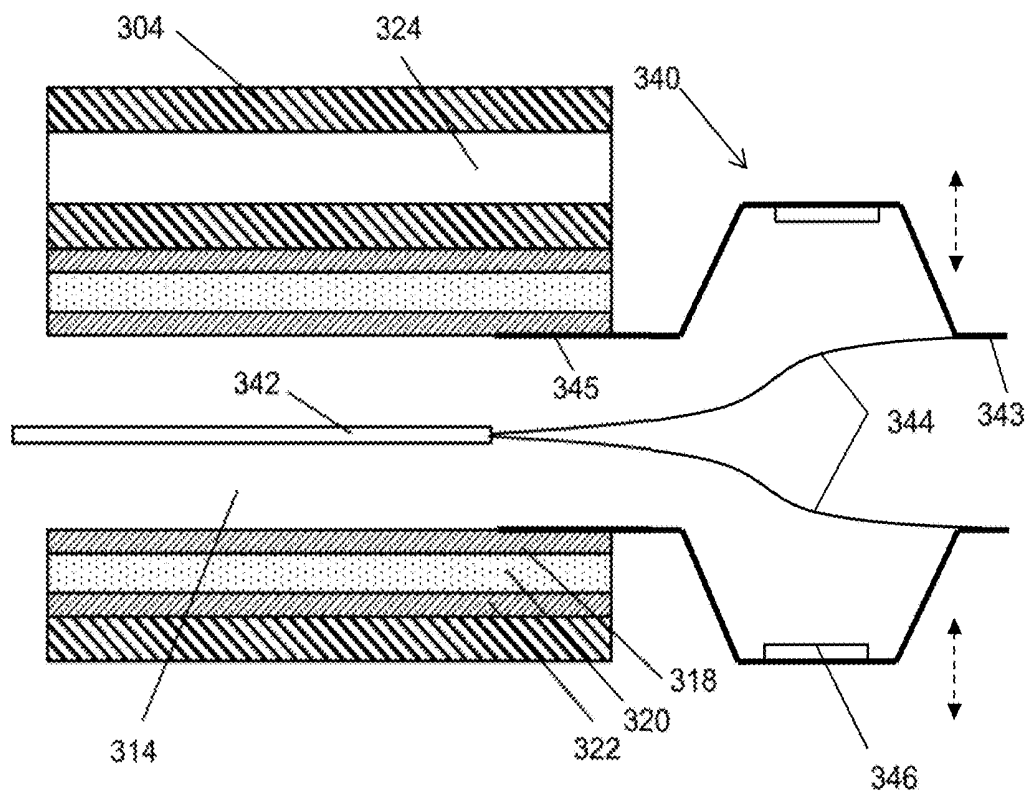


Fig. 15

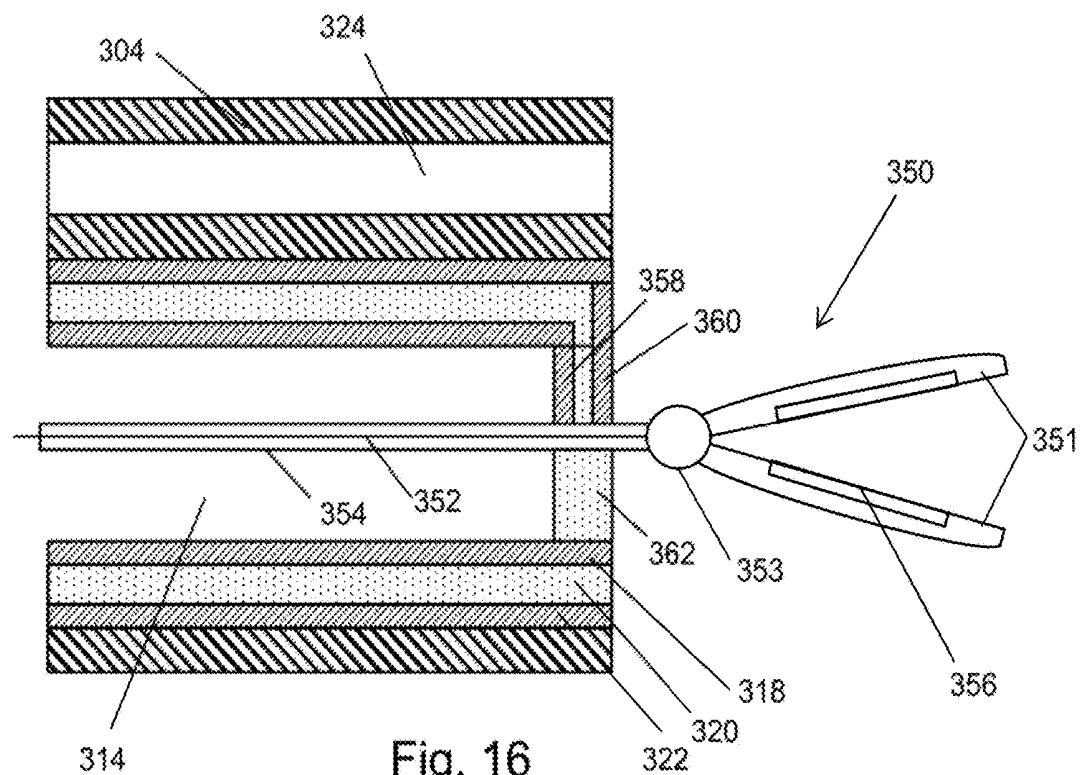


Fig. 16

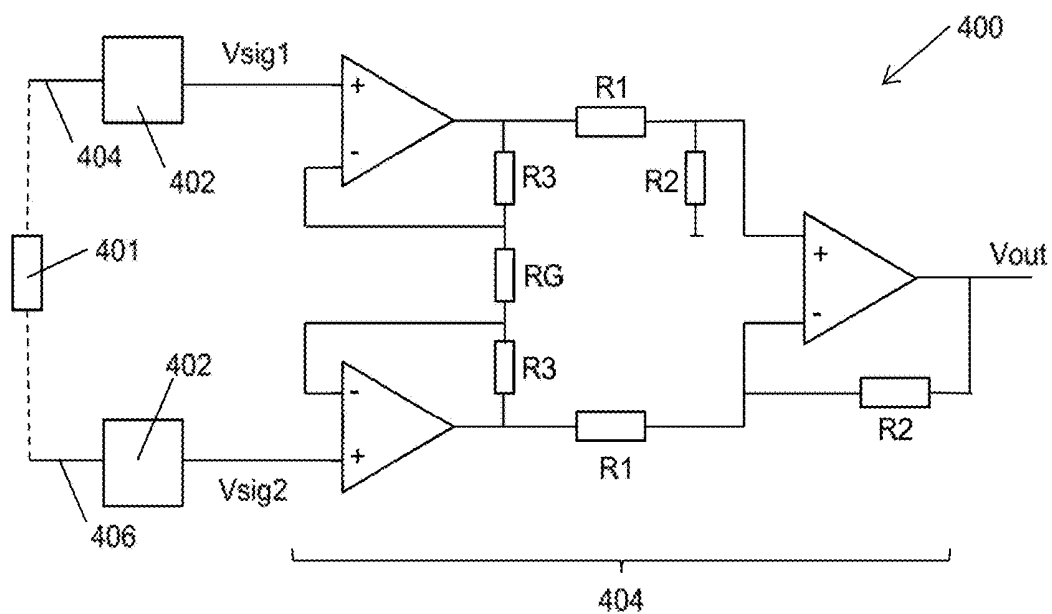


Fig. 19

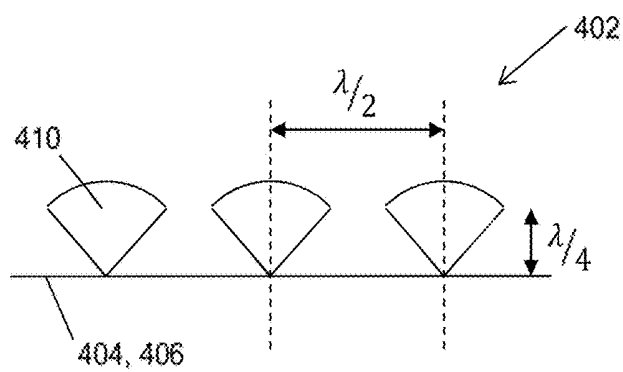


Fig. 20

ELECTROSURGICAL PROBE FOR DELIVERING MICROWAVE ENERGY

FIELD OF THE INVENTION

[0001] The invention relates to an electrosurgical probe for delivering microwave energy to biological tissue in order to ablate the target tissue. In particular, the probe can be used in the lungs or in the uterus, e.g. to ablate tumours, lesions or fibroids and to treat asthma. The probe may be inserted through a channel of a bronchoscope or catheter, or may be used in laparoscopic surgery or open surgery.

BACKGROUND TO THE INVENTION

[0002] It is inherently difficult to gain access to lung tumours due to the small dimensions of the bronchial tree, especially towards the peripheral regions where small nodules are likely to develop. This has resulted in many treatment options being employed such as chemotherapy (targeted medicine, anti-cancer drugs (chemotherapeutic agents)), radiotherapy (delivery of ionizing radiation), surgery (invasive and minimally invasive) and RF/microwave ablation. Surgical procedures involve pneumonectomy (removal of one lung), lobectomy (removal of a lobe), sleeve lobectomy (resection of a lobe along with part of the bronchus that attaches to it), wedge resection (removal of a wedge shaped portion of lung) and segmentectomy/segment resection (resection of a specific lung segment).

[0003] It is known to use microwave emitting probes to treat various conditions in the lungs and other body tissues. For example, in the lungs, microwave radiation can be used to treat asthma and ablate tumours or lesions.

[0004] Existing microwave ablation devices on the market are designed to be inserted percutaneously. However, such devices are difficult to locate percutaneously into a moving lung, which can lead to complications such as pneumothorax and haemothorax (air and blood within the pleural cavity respectively).

[0005] Using a probe to deliver the energy to target tissue is preferable because the radiating portion can be positioned close to the target site and so a high proportion of power can be transmitted to the target site and a lower proportion is lost to the surrounding healthy tissue. This reduces side effects of treatment as well as increasing efficiency.

[0006] Efficient lung cancer treatment through minimally invasive procedures is desirable to reduce the mortality rate of lung cancer patients and to reduce the intraoperative and postoperative complication rate. Probes can be inserted into tissue via laparoscopic surgery, open surgery or via channels in the body such as airways. The least invasive method is the use of channels in the body and this reduces strain put on a patient by the procedure. Catheters or bronchoscopes can be used to help to guide the instrument to the target site and some examples of the mechanisms used are given in US2009/306644.

[0007] In US2014/046174, a microwave ablation catheter is disclosed with a radiating section that is delivered to the target site by a bronchoscope through the airways of a patient.

[0008] Various designs of radiating portions can be used, such as a coaxial cable with a radiating portion on the distal end as in US2014/046174 and the energy delivery device of US2013/324995.

SUMMARY OF THE INVENTION

[0009] At its most general, one aspect of the invention provides an electrosurgical instrument for use in minimally invasive surgical techniques that provides, at a very small scale, a localized microwave field capable of precisely ablating tissue in the lungs. This is done through suitable selection of geometry and material for a radiating distal tip thereof. As explained in more detail below, another aspect of the invention integrates a power delivery structure within the instrument cord of a bronchoscope. Both aspects of the invention can be used in combination with each other and/or in conjunction with a steering control, temperature sensing and vision systems, to provide a practitioner with a rich source of feedback information during treatment.

[0010] According to one aspect of the invention, there is provided an electrosurgical instrument for delivering microwave energy into lung tissue, the electrosurgical instrument comprising: a coaxial cable for conveying microwave energy, the coaxial cable having an inner conductor, an outer conductor, and a first dielectric material separating the inner conductor and outer conductor; and a radiating tip portion disposed at a distal end of the coaxial cable to receive the microwave energy from the coaxial cable, wherein the radiating tip portion comprises: a dielectric tip formed from a second dielectric material that is different from the first dielectric material, and a distal conductive portion of the inner conductor, which extends longitudinally into the dielectric tip, and wherein the second dielectric material has a dielectric constant greater than the first dielectric material, whereby the radiating tip portion is arranged to radiate a localized microwave field for tissue ablation. The instrument is thus a coaxial-based device with a dielectric constant load at its distal end. The distal end of the device is designed to facilitate efficient microwave energy delivery into lung tumour tissue to achieve a localized volume of ablation. The resulting localized, thermally induced tissue damage (ablation zone) occurs as a result of dielectric heating. Other modes of energy delivery may be used. For example, the instrument may comprise conductive material arranged on an outer surface of the dielectric tip to form a microstrip of coplanar transmission line for delivering the microwave energy into biological tissue.

[0011] The instrument may also be configured to deliver radiofrequency (RF) energy.

[0012] The effect of the dielectric tip is to reduce the wavelength of the microwave energy, which allows better impedance matching and control of the resultant ablation profile based on small geometry constraints. For example, the outer diameter of the coaxial cable and radiating tip portion may be equal to or less than 1.9 mm, preferably equal to or less than 1.5 mm. This size enables the instrument to fit down and be manipulated by commercially available bronchoscope instrument channels. As explained below, the instrument may also include its own steering mechanism, which can allow it to be manoeuvred when it extends out from the end of the bronchoscope instrument channel.

[0013] In order to maintain flexibility of the device, the axial length of the dielectric tip is equal to or less than 3 mm, preferably equal to or less than 2 mm. This enables the second dielectric material to be relatively rigid without adversely affecting the flexibility of the instrument, especially at its distal end.

[0014] The microwave energy may be a single stable frequency, e.g. 5.8 GHz. The dielectric constant of the second dielectric material may be selected based on the frequency of the microwave energy such that the axial length of the dielectric tip corresponds to a non-negligible fraction of a wavelength of the microwave energy when propagating in the dielectric tip. Herein, a non-negligible fraction may be equal to or greater than 0.05, preferably more than 0.06. This can ensure that the second dielectric material provides a suitable wavelength-shortening effect. In one embodiment, the dielectric constant of the second dielectric material is equal to or greater than 80. For example, titanium dioxide may be used as the second dielectric material. PTFE or any other dielectric that is low loss at the frequency of the microwave energy may be used for the first dielectric material.

[0015] The radiating tip portion may be arranged to act as a quarter wave impedance transformer to match an input impedance to a tissue load impedance. In other words, the geometry of the radiating tip portion is selected so that the effects of the impedance mismatch are invisible when looking into the transmission line prior to the impedance transformer.

[0016] The radiating tip portion may further comprise an intermediate dielectric element surrounding a proximal part of the distal conductive portion and separating the first dielectric material from the dielectric tip, the intermediate dielectric element being formed from a third dielectric material that is different from the second dielectric material. The third dielectric material may be the same as or different from the first dielectric material. The geometry of the intermediate dielectric element can be selected, e.g. using simulations or the like to facilitate the impedance matching function discussed above.

[0017] An embodiment of the instrument may include a handle at the proximal end of the coaxial cable, e.g. to provide an interface to a suitable electrosurgical generator, and a closed ended catheter/sheath for conveying the coaxial cable and radiating tip portion.

[0018] The localized microwave field may be substantially spherical, e.g. around the radiating tip portion. The shortening of the wavelength of the microwave energy in the dielectric tip may prevent the microwave field from extending or elongating proximally, e.g. back down the length of the coaxial cable. One advantage of a spherical field shape is that it is rotation invariant, so the orientation of the instrument in the instrument channel does not need to be controlled.

[0019] However, in some circumstances an equal field on all sides of the radiating tip portion may not be wanted. Thus, the radiating tip portion may include a field shaping element arranged to direct the microwave field to one side of the radiating tip portion. The field shaping elements may include a choke comprising layers of dielectric and conductive material.

[0020] The field shaping element may be a conductive finger extending longitudinally along a side of an outer surface of the dielectric tip opposite to the side from which the microwave field is directed, the conductive finger being electrically connected to the outer conductor of the coaxial cable. The conductive finger thus acts as a reflector for the field to ensure that a majority of the microwave energy is emitted from one side of the radiating tip portion. The conductive finger preferably extends over a narrow circum-

ferential portion of the dielectric tip. The narrower the circumferential dimension of the conductive finger, the better the impedance matching function.

[0021] The conductive finger preferably extends beyond the distal conductive portion. For example, the radiating tip portion may include a dielectric cap disposed distally to the dielectric tip and distal conductive portion, the conductive finger extending along an outer surface of the dielectric cap, whereby the conductive finger extends further from the coaxial cable than the distal conductive portion. This configuration also improves the impedance matching function. The dielectric cap is formed from a fourth dielectric material that is not the same as the second dielectric material. The fourth dielectric material is preferably a material that exhibits low loss for the microwave energy, and may be the same as the first dielectric material. Thus, the first dielectric material (i.e. the dielectric in the coaxial cable) may be the same as the third dielectric material (which acts as an isolating barrier for the outer conductor at the end of the coaxial cable) and the fourth dielectric material (which can form a distal tip of the device. All of these elements may be formed from PTFE, for example. The second dielectric material can be sandwiched between the third and fourth dielectric materials and has a higher dielectric constant. The second dielectric material can be made from titanium dioxide, for example.

[0022] The conductive finger may be an extension of the outer conductor of the coaxial cable. It may therefore be fixed on the dielectric tip. In this example, the instrument may be needed to be rotatable in the instrument channel in order to control the position of the radiated microwave field.

[0023] However, in another embodiment, the conductive finger may be a distal part of a conductive sleeve mounted on and electrically connected to the outer conductor of the coaxial cable, wherein the conductive sleeve is rotatable relative to the dielectric tip to adjust the circumferential position of the conductive finger. In this arrangement, the whole instrument does not need to be rotatable in the instrument channel. Only the conductive sleeve needs to be controlled. The orientation of the conductive sleeve may be controlled by a pair of guide wires or the like.

[0024] The conductive sleeve may be used to provide other types of field shaping element. For example, the field shaping element may be a conductive sleeve formed over the dielectric tip, the conductive sleeve having a radiating slot formed therein on the side from which the microwave field is directed. The conductive sleeve may be rotatable relative to the dielectric tip to adjust the circumferential position of the radiating slot.

[0025] The conductive sleeve does not need to rotate. For example, the conductive sleeve may have a plurality of radially offset radiating slots around the outer surface of the dielectric tip, and the radiating tip portion may comprise an actuator operable to selectively expose only one of the plurality of radiating slots. In an embodiment, the conductive sleeve may have a pair of radiating slots on opposite sides of the dielectric tip. The actuator may comprise a longitudinally slidable sleeve having radially offset (e.g. diametrically opposed) cut outs formed therein, wherein the actuator is movable between a first position in which a first cut out exposes a first one of the pair of radiating slots and a second position in which a second cut out exposes a second one of the pair of radiating slots. The relative positions of the cut outs and radiating slots is chosen to prevent both

radiating slots from being exposed at the same time. For example the cut outs may be offset from one another in a longitudinal direction. In this example, the pair of radiating slots may be laterally aligned or offset by a different amount in order to avoid simultaneous exposure. In an embodiment, the actuator may be movable to a third position in which both slots are exposed, e.g. to enable a spherical field to be emitted.

[0026] The field shaping element may include a patch antenna formed on the dielectric tip. Alternatively, the field shaping element may comprise a leaky slotted line, i.e. a radiating element formed by providing a plurality of slots in the ground plane of a coaxial transmission line.

[0027] An outer sheath may be formed over the radiating tip portion, e.g. to provide biocompatibility and/or protect the instrument. The dielectric tip may have a geometry that assists manipulation of the instrument within the lung. For example, the distal end of the device may be rounded, e.g. dome-like or hemispherical.

[0028] The instrument may comprise an imaging element for conveying an imaging signal to permit visualisation of a distal end of the instrument. In an embodiment, the imaging element may include a fibrescope comprising a bundle of optical fibres. The bundle of optical fibres may have a diameter of 0.3 mm to 0.5 mm, and may contain both illumination and detection fibres. Suitable fiberscopes are manufactured by Fujikura and can provide images with up to 10,000 pixels. The inner conductor and distal conductive portion may be hollow to define a channel for carrying the bundle of optical fibres. Alternatively, the bundle of optical fibres may be integrally formed with the inner conductor and distal conductive portion. For example, the bundle of fibres may extend through the first dielectric material and radiating tip portion and may have a layer of conductive material over its outer surface, whereby it actually forms the inner conductor of the coaxial cable and the distal conductive portion.

[0029] In an alternative embodiment, the imaging element may comprise an image sensor mounted at the distal end of the radiating tip portion and a communication cable for conveying a signal from the image sensor to the proximal end of the instrument. The image sensor may be CMOS- or CCD-based. The communication cable may include one or more optical fibres for conveying an illumination signal. In another embodiment, the image sensor may include an ultrasound transducer. Similarly to the arrangement discussed above, the inner conductor and distal conductive portion may be hollow to define a channel for carrying the communication cable.

[0030] In other embodiments, the bundle of optical fibres or communication cable may be offset from the axis of the coaxial cable. For example, the bundle of optical fibres or the communication cable may run alongside the coaxial cable or may be integrated within an outer sheath or catheter that surrounds the instrument.

[0031] In order to obtain better image resolution, there may be a plurality of image sensors mounted at the distal end of the instrument. A plurality of optical fibre bundles may convey the image data to the proximal end of the instrument.

[0032] The instrument may further include a temperature sensor at the distal end thereof. The instrument can therefore provide additional feedback about the conditions at the distal end of the instrument. The temperature sensor may be a thermocouple mounted on the outer conductor of the coaxial cable. The thermocouple may have a plurality of stubs

formed therewith, the stubs being arranged to filter out a signal having the same frequency as the microwave energy.

[0033] Alternatively, the temperature sensor may be combined with the imaging element discussed above. For example, the temperature sensor may include a temperature sensitive micromechanical structure at the distal end of the end. The imaging element or some other means may be used to optically monitor the temperature sensitive micromechanical structure and thereby derive information indicative of temperature conditions at the distal end of the instrument.

[0034] The microwave energy may be applied in a pulsed manner. To avoid the microwave energy from swamping response signal from the temperature sensor, temperature measurements may be taken when the microwave energy is off, i.e. in an OFF period of the pulsed operation. Alternatively or additionally, the instrument may include a filtering arrangement for removing noise on the response signal from the temperature sensor caused by the microwave energy. The filtering arrangement may include a low pass filter and a common mode injection instrumentation amplifier arranged to remove higher frequency components from the response signal.

[0035] The whole instrument may be mounted in a closed end catheter or outer sheath. The outer sheath may be a multi lumen catheter arranged to convey any one or more of: guide wires for controlling movement of the radiating tip section, and fluid for cooling the distal end of the instrument. By providing guide wires to control movement of the instrument, it may be possible to navigate inside the bronchial tree to locate and treat tumours that cannot currently be treated. The guide wires may run inside the outer sheath or can be extruded as an integral part of it. One, two or three guide wires may be used.

[0036] In another aspect, the invention provides an electrosurgical apparatus for delivering microwave energy into lung tissue, the electrosurgical apparatus comprising: a generator for generating microwave energy; a bronchoscope for non-percutaneous insertion into a patient's lungs, the bronchoscope having an instrument channel running along its length; and an electrosurgical instrument as set out above in the instrument channel of the bronchoscope, wherein the coaxial cable is connected to receive microwave energy from the generator. The generator may be arranged to deliver pulses of microwave energy in time with the breathing cycle of the patient.

[0037] In a further aspect, the invention provides a bronchoscope comprising: a body; and a flexible instrument cord for non-percutaneous insertion to a patient's lungs, the instrument cord extending from the body and having an longitudinally extending instrument channel formed therethrough, wherein the body includes: a power input port that is connectable to receive microwave energy, and an optical port arranged to receive optical signals from a distal end of the instrument cord, and wherein the instrument cord comprises a coaxial transmission line formed around the instrument channel, the coaxial transmission line being connected to the power input port to convey microwave energy to the distal end of the instrument cord. In this aspect, the means for delivery power is integrated into the instrument cord of the bronchoscope as opposed to being delivered in a coaxial cable that runs through the instrument channel thereof. This enables a large coaxial structure to be used within the same

overall instrument cord diameter. In turn this can reduce losses and/or free up space in the instrument channel for other uses.

[0038] The bronchoscope may have a radiator mounted at a distal end of the instrument channel, the radiator being electrically connected to the coaxial transmission line to receive microwave energy therefrom and emit a microwave field. The radiator may be an electrosurgical instrument as described above, e.g. with a section of coaxial cable that protrudes from the instrument cord and terminates at a radiating tip. The outer diameter of the coaxial transmission line may be greater than the outer diameter of the coaxial cable in the electrosurgical instrument. In other word the overall power delivery structure comprises a pair of coaxial lines having differing diameters.

[0039] The bronchoscope with integrated coaxial transmission line may be used with other types of radiator. For example, the radiator may comprise any one of: an expandable balloon, a radially expanding tube, a forceps structure, and a paddle structure.

[0040] The instrument channel (or another dedicated channel in the instrument cord) may be arranged to receive fluid (e.g. a coolant such as saline or water) for cooling the coaxial transmission line during treatment. The body may therefore comprise a fluid input port, the fluid input port being in communication with the instrument channel (or another lumen in the instrument cord).

[0041] The body may include a control actuator connected to one or more guide wires, the guide wires extending through the instrument cord to the radiator, wherein the control actuator is operable to move the guide wires within the instrument cord to control movement of the radiator. The guide wires may extend through the instrument channel or through other dedicated passageways in the instrument cord.

[0042] The body may include an illumination port and the instrument cord may include one or more optical channels in optical communication with the illumination port for conveying an illumination signal to the distal end thereof to illuminate a treatment region. The illumination signal may be optical radiation (e.g. white light) for enabling the treatment region to be viewing through the optical port (e.g. eye piece). Alternatively or additionally, the illumination signal may enable images of the treatment region to be captured.

[0043] In one example, the illumination signal may be for spectroscopic purposes. It may be from a UV laser, for example.

[0044] A light source may be mounted to the body to generate the illumination signal. The light source may be an LED or halogen light source.

[0045] In another aspect, the invention provides an electrosurgical apparatus for delivering microwave energy into lung tissue, the electrosurgical apparatus comprising: a generator for generating microwave energy; and a bronchoscope as described above, wherein the power input port is connected to the generator to convey the microwave energy to the coaxial transmission line. The generator may be arranged to pulse the microwave energy with a duty cycle between 1% and 50%.

[0046] Herein, radiofrequency (RF) may mean a stable fixed frequency in the range 10 kHz to 300 MHz and microwave frequency may mean a stable fixed frequency in the range 300 MHz to 100 GHz. Preferred spot frequencies for the RF energy include any one or more of: 100 kHz, 250

kHz, 400 kHz, 500 kHz, 1 MHz, and 5 MHz. Preferred spot frequencies for the microwave energy include 915 MHz, 2.45 GHz, 5.8 GHz, 14.5 GHz, and 24 GHz.

[0047] Herein, the term “conductive” means “electrically conductive” unless the context dictates otherwise.

BRIEF DESCRIPTION OF DRAWINGS

[0048] Examples of the invention are described in more detail below with reference to the accompanying drawings, in which:

[0049] FIG. 1 is a schematic diagram of an electrosurgical apparatus with which the present invention can be used;

[0050] FIG. 2 is a longitudinal cross section of a electrosurgical device that can be used in embodiments of the invention;

[0051] FIG. 3 is a longitudinal cross section of an electrosurgical device that is an embodiment of the invention;

[0052] FIG. 4 is a longitudinal cross section of an electrosurgical device that is an embodiment of the invention;

[0053] FIG. 5A is a longitudinal cross section of a simulation of the radiation absorption pattern produced by the electrosurgical device of FIG. 1;

[0054] FIG. 5B is an axial cross section of a simulation of the radiation absorption pattern produced by the electrosurgical device of FIG. 1;

[0055] FIG. 6 is a longitudinal cross section of a simulation of the radiation absorption pattern produced by the electrosurgical device of FIG. 3;

[0056] FIG. 7A is a first longitudinal cross section of a simulation of the radiation absorption pattern produced by the electrosurgical device of FIG. 4;

[0057] FIG. 7B is an axial cross section of a simulation of the radiation absorption pattern produced by the electrosurgical device of FIG. 4;

[0058] FIG. 7C is a second longitudinal cross section of a simulation of the radiation absorption pattern produced by the electrosurgical device of FIG. 4;

[0059] FIG. 8A is a longitudinal cross section of an electrosurgical device that is an embodiment of the invention;

[0060] FIG. 8B is a schematic isometric view of a first variant of the electrosurgical device shown in FIG. 8A;

[0061] FIG. 8C is a schematic isometric view of a second variant of the electrosurgical device shown in FIG. 8A;

[0062] FIG. 9A is a longitudinal cross section of an electrosurgical device that is an embodiment of the invention;

[0063] FIG. 9B is a schematic isometric view of the electrosurgical device shown in FIG. 9A;

[0064] FIG. 10A is a longitudinal cross section of an electrosurgical device that is an embodiment of the invention;

[0065] FIG. 10B is a schematic isometric view of the electrosurgical device shown in FIG. 10A is a first configuration;

[0066] FIG. 10C is a schematic isometric view of the electrosurgical device shown in FIG. 10A is a second configuration;

[0067] FIG. 11 is a schematic view of a bronchoscope with integrated power delivery that is an embodiment of the invention;

[0068] FIG. 12 is a schematic view along the axis of the instrument cord of the bronchoscope shown in FIG. 11;

[0069] FIG. 13 is a schematic cross-sectional through a distal portion of the instrument cord of a bronchoscope that is a first variant of the embodiment shown in FIG. 11;

[0070] FIG. 14 is a schematic cross-sectional through a distal portion of the instrument cord of a bronchoscope that is a second variant of the embodiment shown in FIG. 11;

[0071] FIG. 15 is a schematic cross-sectional through a distal portion of the instrument cord of a bronchoscope that is a third variant of the embodiment shown in FIG. 11;

[0072] FIG. 16 is a schematic cross-sectional through a distal portion of the instrument cord of a bronchoscope that is a fourth variant of the embodiment shown in FIG. 11;

[0073] FIG. 17 is a schematic cross-sectional through a distal portion of the instrument cord of a bronchoscope that is a fifth variant of the embodiment shown in FIG. 11;

[0074] FIG. 18 is a schematic cross-sectional through a distal radiator that can be used with the embodiment shown in FIG. 11;

[0075] FIG. 19 is a schematic circuit diagram for an instrumentation amplifier that can be used with the distal radiator of FIG. 18; and

[0076] FIG. 20 is a schematic diagram of a low pass filter that that can be used with the distal radiator of FIG. 18.

DETAILED DESCRIPTION; FURTHER OPTIONS AND PREFERENCES

[0077] FIG. 1 is a schematic diagram of a complete electrosurgery system 100 that is capable of supplying microwave energy and fluid, e.g. cooling fluid, to the distal end of an invasive electrosurgical instrument. The system 100 comprises a generator 102 for controllably supplying microwave energy. A suitable generator for this purpose is described in WO 2012/076844, which is incorporated herein by reference. The generator may be arranged to monitor reflected signals received back from the instrument in order to determine an appropriate power level for delivery. For example, the generator may be arranged to calculate an impedance seen at the distal end of the instrument in order to determine an optimal delivery power level. The generator may be arranged to deliver power in a series of pulses which are modulated to match a patient's breathing cycle. This will allow for power delivery to occur when the lungs are deflated.

[0078] The generator 102 is connected to an interface joint 106 by an interface cable 104. The interface joint 106 is also connected to receive a fluid supply 107 from a fluid delivery device 108, such as a syringe. If needed, the interface joint 106 can house an instrument control mechanism that is operable by sliding a trigger 110, e.g. to control longitudinal (back and forth) movement of one or more control wires or push rods (not shown). If there is a plurality of control wires, there may be multiple sliding triggers on the interface joint to provide full control. The function of the interface joint 106 is to combine the inputs from the generator 102, fluid delivery device 108 and instrument control mechanism into a single flexible shaft 112, which extends from the distal end of the interface joint 106.

[0079] The flexible shaft 112 is insertable through the entire length of an instrument (working) channel of a bronchoscope 114.

[0080] The flexible shaft 112 has a distal assembly 118 (not drawn to scale in FIG. 1) that is shaped to pass through the instrument channel of the bronchoscope 114 and protrude (e.g. inside the patient) at the distal end of the

bronchoscope's tube. The distal end assembly includes an active tip for delivering microwave energy into biological tissue. The tip configuration is discussed in more detail below.

[0081] The structure of the distal assembly 118 discussed below may be particularly designed for use with a conventional steerable flexible bronchoscope, whereby the maximum outer diameter of the distal assembly 118 is equal to or less than 2.5 mm, and preferably less than 1.9 mm (and more preferably less than 1.5 mm) and the length of the flexible shaft can be equal to or greater than 1.2 m.

[0082] The apparatus described above is one way of introducing the instrument. Other techniques are possible. For example, the instrument may also be inserted using a catheter.

[0083] The invention seeks to provide an instrument that can deliver microwave energy to tissue, particularly to the lungs. In order for side effects to be reduced and the efficiency of the instrument to be maximised, the transmitting antenna should be located as close to the target tissue as possible. Ideally, the radiating part of the instrument is located inside (e.g. at the centre of) the tumour during treatment. In order to reach the target site within the lungs, the instrument will need to be guided through the airways and around obstacles such as the vocal chords. This means that the instrument will ideally be flexible and have a small cross section. Particularly, the instrument should be very flexible near the antenna where it needs to be steered along bronchioles which can be narrow and winding. The size of the antenna part of the instrument should also be reduced where possible to allow the antenna to work properly in small locations and increase flexibility of the instrument when components of the antenna are rigid. As discussed below, the instrument may comprise two coaxial transmission lines arranged in series, with a proximal coaxial transmission line having a greater outer diameter than a distal coaxial transmission line. The outer diameter of the proximal coaxial transmission line may be equal to or greater than 2 mm and the outer diameter of the distal coaxial transmission line may be equal to or less than 1.5 mm, e.g. 1.2 mm. The proximal coaxial transmission line may extend along the majority of the flexible shaft. For example, proximal coaxial transmission line may have a length of 1 m and the distal coaxial transmission line may have a length equal to or less than 0.3 m. This arrangement can ensure that more microwave power is delivered into the tissue without the proximal coaxial transmission line getting too hot.

[0084] Another way of avoiding unwanted heating of the cable is to deliver the microwave energy in a pulsed manner. In one example, the microwave energy can be delivered with a duty cycle of 9%, e.g. a 110 ms period consisting of a 10 ms ON portion and a 100 ms OFF portion. The duty cycle may be less than 9%, e.g. 5%.

[0085] Heating of the cable can also be mitigated by providing cooling fluid.

[0086] The cable for delivering the microwave radiation to the target site should be low-loss, have a small cross-section and be flexible. The cable should be low loss to avoid heating during treatment and so that there is enough power at the distal end to produce the desired radiation from the antenna.

[0087] If the cable is not separated from the body by the use of a sealed bronchoscope, catheter or other protective

sheath when in use, then the cable should be made of biologically inert material to avoid unwanted interaction with the body.

[0088] A preferred cable type is a coaxial cable which is made up of an inner conductor axially surrounded by a dielectric sheath which is in turn axially surrounded by an outer conductor. The radiating portion in an antenna produced from such a cable may be made up of a section of inner conductor and dielectric sheath which protrudes from the end of the outer conductor of the coaxial cable.

[0089] The invention also seeks to provide an antenna with a well-defined radiation pattern. It is desirable that a practitioner would be able to select an instrument for the treatment of a specific area of tissue, such that the radiation of target tissue is maximised and the radiation of healthy tissue is minimised. For example, in some circumstances it can be desirable to produce a generally spherically symmetric radiation pattern with a substantially uniform power absorption distribution, so that the amount of radiation received by an area of tissue can be more easily controlled by the practitioner. However, in other circumstances it may also be desirable to restrict the radiation to one side of the instrument, to avoid unnecessary radiation of healthy tissue on the other side of the instrument. For example, such a configuration may be used when the target tissue is on only one side of the airway in which the instrument is positioned for treatment.

[0090] It is also preferable that the instrument can be operated alongside other instruments to enable practitioners to receive information from the target site. For example, a bronchoscope may aid the steering of the instruments around obstacles such as the vocal chords. Other instruments may include a thermometer or camera.

[0091] In the following description, unless stated otherwise, the length of a component refers to its dimension in the direction parallel to the longitudinal axis of the coaxial cable.

[0092] FIG. 2 is a longitudinal cross section taken along the axis of a coaxial cable which forms a tissue ablation antenna 10. The tissue ablation antenna comprises a radiating portion 12. The inner conductor 14 is radially surrounded by the dielectric sheath 16 which is in turn radially surrounded by the outer conductor 18. The inner conductor 14 and the insulating sheath 16 extend beyond a distal end 19 of the outer conductor 18 and the protruding section of inner conductor and insulating sheath forms the radiating portion 12. In this example, the inner conductor 14 is shorter than the insulating sheath 16 so that the end of the insulating sheath 16 forms a cap over the inner conductor 14.

[0093] FIGS. 5A and 5B show longitudinal and axial cross-sections respectively of a radiation pattern simulation for the antenna 10 shown in FIG. 2. It can be seen that the pattern covers an elongated region near the end of the outer conductor 18. It is axially symmetric and is generally strongest at the distal end 19 of the outer conductor 18.

[0094] FIG. 3 is a cross-sectional view of the distal end of an electrosurgical instrument 200 that is an embodiment of the invention. The electrosurgical instrument 200 comprises a coaxial cable 202 that is connected at its proximal end to a electrosurgical generator (not shown) in order to convey microwave energy. The coaxial cable 202 comprises an inner conductor 206, which is separated from an outer conductor 208 by a first dielectric material 210. The coaxial cable 202 is preferably low loss for microwave energy. A

choke (not shown) may be provided on the coaxial cable to inhibit back propagation of microwave energy reflected from the distal end and therefore limit backward heating along the device.

[0095] The device may include a temperature sensor at the distal end. For example, in FIG. 3 a thermocouple 230 is mounted on the outer conductor to transmit a signal back to the proximal end that is indicative of temperature at the distal end of the instrument. This type of temperature sensor is discussed in more detail below with reference to FIGS. 18 to 20.

[0096] Other techniques for temperature monitoring can be used. For example, one or more micromechanical structure whose physical configuration is sensitive to temperature may be mounted in the distal portion of the device, e.g. in or on the outer sheath discussed below. These structures can be interfaced with an optical fibre, whereby changes in a reflected signal caused by movement of the structure can be indicative of temperature changes.

[0097] The coaxial cable 202 terminates at its distal end with a radiating tip section 204. In this embodiment, the radiating tip section 204 comprises a distal conductive section 212 of the inner conductor 206 that extends before a distal end 209 of the outer conductor 208. The distal conductive section 212 is surrounded at its distal end by a dielectric tip 214 formed from a second dielectric material, which is different from the first dielectric material 210. The length of the dielectric tip 214 is shorter than the length of the distal conductive section 212. An intermediate dielectric sleeve 216 surrounds the distal conductive section 212 between the distal end of the coaxial cable 202 and the proximal end of the dielectric tip 214. The intermediate dielectric sleeve 216 is formed from a third dielectric material, which is different from the second dielectric material but which may be the same as the first dielectric material 210.

[0098] In this embodiment, the coaxial cable 202 and radiating tip section 204 have an outer sheath 218 formed over their outermost surfaces. The outer sheath 218 may be formed from a biocompatible material. The outer sheath 218 has a thickness that is small enough to ensure that it does not significantly interfere with the microwave energy radiated by the radiating tip section 204 (i.e. radiating pattern and return loss). In an embodiment, the sheath is made from PTFE, although other materials are also appropriate. The thickness of the wall of the sheath is selected to be withstand breakdown voltages equal to or greater than 500 V (peak).

[0099] The purpose of the dielectric tip 214 is to alter the shape of the radiated energy. The second dielectric material is selected to reduce the wavelength of the microwave energy, which results in the radiated energy exhibiting a more spherical radiation pattern. To do this, the second dielectric material preferably has a large dielectric constant (relative permittivity). The dielectric constant of the second dielectric material is preferably chosen to enable the length of the dielectric tip 214 to be minimised whilst still constituting a non-negligible portion of a wavelength of the microwave energy when it propagates through the second dielectric material. It is desirable for the dielectric tip to be as short as possible in order to retain flexibility in the device, especially if the second dielectric material is rigid. In an embodiment, the dielectric tip may have a length equal to or less than 2 mm. The dielectric constant of the second dielectric material may be greater than 80, and is preferably

100 or more at the frequency of the microwave energy. The second dielectric material may be TiO_2 (titanium dioxide).

[0100] The wavelength of radiation in a material becomes shorter as the dielectric constant of the material increases. Therefore a dielectric tip **214** with a greater dielectric constant will have a greater effect on the radiation pattern. The larger the dielectric constant, the smaller the dielectric tip **214** can be while still having a substantial effect on the shape of the radiation pattern. Using a dielectric tip **214** with a large dielectric constant means that the antenna can be made small and so the instrument can remain flexible. For example the dielectric constant in TiO_2 is around 100. The wavelength of microwave radiation having a frequency of 5.8 GHz is about 6 mm in TiO_2 compared to around 36 mm in PTFE (which may be the material used for the first and/or third dielectric materials). A noticeable effect on the shape of the radiation pattern can be produced in this arrangement with a dielectric tip **214** of approximately 1 mm. As the dielectric tip **214** is short, it can be made from a rigid material whilst still maintaining flexibility of the antenna as a whole. The dielectric tip **214** may have any suitable distal shape. In FIG. 3 it has a dome shape, but this is not necessarily essential. For example, it may be cylindrical, conical, etc. However, a smooth dome shape may be preferred because it increases the mobility of the antenna as it is manoeuvred through small channels. The dielectric tip **214** may be coated with a non-stick material such as Parylene C or Parylene D, or PTFE to prevent the tissue from sticking to the instrument. The whole instrument can be coated in this way.

[0101] The properties of the intermediate dielectric sleeve **216** are preferably chosen (e.g. through simulation or the like) so that the radiating tip section **204** forms a quarter wave impedance transformer for matching the input impedance of the generator into a biological tissue load in contact with the radiating tip section **204**.

[0102] A longitudinal cross section of a simulation of the absorption pattern of an antenna having the configuration shown in FIG. 3 is shown in FIG. 6. The pattern produced is more uniform and more spherical than the pattern shown in FIGS. 5A and 5B. The pattern in FIG. 6 is axially symmetric and more of the radiation is concentrated around the radiating portion rather than spreading down the cable as occurs in FIGS. 5A and 5B. This means that, when in use, an area of tissue may be radiated more uniformly, meaning there is less chance of damage to healthy tissue. The radiation is also less spread out, allowing the practitioner to more accurately radiate target tissue and reduce radiation of or damage to healthy tissue. The pear drop shape of radiation pattern shown in FIG. 6 may also be particularly useful for treating fibroids.

[0103] During treatment, the surrounding tissue absorbs the radiated energy. The volume of tissue into which the energy is delivered depends on the frequency of the microwave energy.

[0104] FIG. 4 is a cross-sectional view of the distal end of an electrosurgical instrument **220** that is another embodiment of the invention. Components in common with electrosurgical instrument **200** shown in FIG. 3 are given the same reference numbers and are not described again.

[0105] In this embodiment the radiating tip section **204** is configured differently. The intermediate dielectric sleeve **216** is a short collar having a length much less than the dielectric tip **214**. However, the dielectric tip **214** acts in the

same manner as described above with respect to FIG. 3 in that it shortens the wavelength of the microwave energy to provide a more focussed field.

[0106] A dielectric cap **222** formed of a fourth dielectric material, which is different from the second dielectric material but may be the same as the first or third dielectric material **210** is formed at the distal end of the dielectric tip **214**. Similarly to FIG. 3, the second dielectric material may be TiO_2 and the third dielectric material may be PTFE. The fourth dielectric material may also be PTFE.

[0107] FIG. 4 is not drawn to scale. The length of the dielectric tip **214** may be similar to that discussed above, e.g. less than 3 mm, preferably less than 2 mm. The length of the dielectric cap **222** may be shorter than the length of the dielectric tip **214**. For example, it may be equal to or less than 1 mm. In both FIGS. 3 and 4 it is desirable for the maximum outer diameter of the instrument to be equal to or less than 3 mm, preferably equal to or less than 1.9 mm, although the invention need not be limited to these dimensions.

[0108] In this embodiment a portion of the outer conductor **208**, e.g. a narrow strip or conductive finger **224** extends beyond the coaxial cable **202**. The conductive finger **224** acts as a field reflector to cause the radiating field to be directed out of the side of the radiating tip that is opposite to the conductive finger **224**.

[0109] The dielectric cap **222** is provided to enable the conductive finger to extend beyond the distal end of the distal conductive portion **212** formed by the inner conductor **206**. This configuration has been found to improve the impedance matching function of the radiating tip section **204**.

[0110] In a specific example of the structure shown in FIG. 4, the conductive finger **224** may extend by a length of 3.6 mm beyond the distal end of the coaxial cable. The dielectric tip **214** may have a length of 2.5 mm and may be made from TiO_2 . The distal conductive portion **212** of the inner conductor **206** may protrude 2.6 mm from the end of the coaxial cable **202**, so the intermediate dielectric sleeve **216** may have a length of 0.1 mm. With this configuration, the conductive finger **224** extends 1 mm past the distal end of the distal conductive portion **212**, which improves the effectiveness of its reflecting function. The dielectric cap **222** has a length of 1 mm. The dimensions given here relate to a specific example that is based on a certain dielectric constant value. For other dielectric materials, the dimensions may change accordingly.

[0111] As this antenna is so short, it is easier to introduce into tightly curved tubes and can be guided through small lung airways to get close to target sites.

[0112] FIGS. 7A, 7B and 7C shows various views of simulated absorption of microwave energy radiated by the antenna structure shown in FIG. 4.

[0113] FIG. 7A shows a longitudinal cross section of the simulated absorption. Much more radiation is emitted from the side of the antenna that is opposite to the conductive finger **224**. FIG. 7B shows an axial view of the simulated absorption that shows a similar effect.

[0114] FIG. 7C shows a longitudinal cross section of the simulated absorption when looking directly at the side opposite the conductive finger, which shows how the shape of the field is changed by the choice of material for the dielectric tip **214**.

[0115] FIG. 8A is a cross-sectional view of the distal end of an electrosurgical instrument **240** that is another embodiment of the invention. Components in common with electrosurgical instrument **220** shown in FIG. 4 are given the same reference numbers and are not described again.

[0116] In this embodiment the conductive finger **224** is not provided as an extension of the outer conductor **208**. Instead, it is formed as part of an electrically conductive sleeve **242** that is mounted over at least a distal portion of the coaxial cable **202**. The electrically conductive sleeve **242** is electrically connected to the outer conductor **208**, e.g. by an interference fit. In this embodiment, the electrically conductive sleeve **242** is rotatable relative to the coaxial cable **202** and radiating tip section **204**. This allows the location of the conductive finger **224** to be varied around the circumference of the radiating tip section without having to twist the whole instrument.

[0117] The conductive finger **224** may be configured in various ways. FIG. 8B shows a first variant, in which the conductive finger **224** surrounds a majority of the circumference of the radiating tip section **204**, thereby defining a longitudinal slot **244** through which the dielectric tip **214** is exposed to enable the microwave energy to be radiated.

[0118] FIG. 8C shows a second variant, in which the conductive finger **224** is a narrow elongate strip extending from the rest of the electrically conductive sleeve **242**.

[0119] FIG. 9A is a cross-sectional view of the distal end of an electrosurgical instrument **250** that is another embodiment of the invention. Components in common with electrosurgical instrument **240** shown in FIG. 8A are given the same reference numbers and are not described again.

[0120] In this embodiment, instead of defining the conductive finger **224**, the rotatable electrically conductive sleeve **242** extends to the distal end of the radiating tip section **204** but has one or more slots **246** (two in this example) formed in it to expose the dielectric tip **214** to enable the microwave energy to be radiated. FIG. 9B illustrates the outward appearance of this arrangement.

[0121] If the distal end of the instrument is arranged as an open circuit, the slots may be located at multiples of a half wavelength of the microwave energy from the distal end. If the distal end is arranged as a short circuit, the distal-most slot would be located at a quarter wavelength of the microwave energy from the distal end, with subsequent slots being separated from the first slot by multiples of a half wavelength of the microwave energy. Where the slot lies over the second dielectric material, it is the reduced wavelength of the microwave energy in that dielectric material that is used to calculate the position of the slots.

[0122] In another variant of this embodiment, the rotatable electrically conductive sleeve is omitted and instead the outer conductor extends to cover the radiating tip section **214** and the slot(s) are formed in the outer conductor.

[0123] In other unillustrated embodiments, different types of radiating structure may be provided at the radiating tip section **204** to enable microwave energy to be launched into tissue. For example, patch antennas could be provided by fabricating conductive structures on, e.g. partially metallizing, the outer surface of the dielectric tip **214**. Alternatively, the dielectric tip **214** may be configured to include a microstrip line or coplanar antenna structure that is connected to receive power from the coaxial cable **102**.

[0124] FIG. 10A is a cross-sectional view of the distal end of an electrosurgical instrument **260** that is another embodi-

ment of the invention. Components in common with electrosurgical instrument **240** shown in FIG. 8A are given the same reference numbers and are not described again.

[0125] In this embodiment the outer conductor **208** extends to the distal end of the radiating tip section **204** and has a pair of diametrically opposed slots **256a**, **256b** formed therein to expose the dielectric tip **214**. An axially slidable electrically conductive sleeve **252** is mounted over at least a distal portion of the coaxial cable **202** and the radiating tip section **204**. The electrically conductive sleeve **252** is conductively connected to the outer conductor **208** such that they are effectively the same conductive body. The electrically conductive sleeve **252** has a pair of slots **254a**, **254b** formed on opposite sides thereof. However, unlike the slots **256a**, **256b** on the outer conductor **208**, the slots **254a**, **254b** are axially offset from each other. Each of the slots **254a**, **254b** is circumferentially aligned with a respective one of the slots **256a**, **256b**, so that the dielectric tip can be exposed when each slot **254a**, **254b** is axially aligned with its respective slot. Accordingly, in use, the axial position of the electrically conductive sleeve **252** can be selected so that only one of the slots **256a**, **256b** is in line with its respective slot **254a**, **254b**, whereby the lateral direction in which microwave energy is radiated from the dielectric tip can be selected using a purely axial (longitudinal) actuation motion.

[0126] FIG. 10B shows the axially slidable electrically conductive sleeve **252** in a forward position in which its rearward slot **256b** is aligned with a first slot **254b** on the outer conductor **208**. FIG. 10C shows the axially slidable electrically conductive sleeve **252** in a retracted position in which its forward slot **256a** is aligned with a second slot **254a** on the outer conductor **208**.

[0127] The axially slidable electrically conductive sleeve **252** may be moved between the forward and retracted positions by control wires or push rods (not shown) that pass along the instrument channel of the bronchoscope to an actuator (not shown) at the proximal end of the instrument channel.

[0128] In any of the embodiments discussed above, it may be desirable to include a vision system. For example, it is possible to incorporate one or more imaging components to enable images of the distal end to be transmitted for display to an operator. The image components may include imaging and light bundle optical fibres that perform the function of a fibroscope, i.e. allowing visual imagery to be coupled from the distal end of the device to the proximal for connection to a processing unit via a communication cable.

[0129] In an embodiment, a fibroscope-based vision system may be realised by forming an optical fibre bundle and an image fibre bundle along the length of the instrument. A lens may be provided at the distal end of the fibre bundle to focus the light and image appropriately. The fibre bundle may be metallized on its outer diameter whereby it can also provide the function of the inner conductor of a coaxial based structure. Alternatively the fibre bundle can be placed alongside the coaxial cable within a protective outer sheath. A third construction method could be to incorporate the fibre bundle into the wall thickness of the outer sheath.

[0130] In another embodiment a vision system can be realised using an image sensor (e.g. a suitable CCD/CMOS device) mounted at the distal end of the device, with a communication cable running along the length of the device. A separate illumination fibre bundle or light sources (e.g. LEDs) in the distal end of the device can illuminate the

target in order for the image sensor to capture an image. In this embodiment the communication cable may run within or be integrally formed with the inner conductor of the coaxial cable. Alternatively, it may run externally adjacent to the coaxial cable or within the wall thickness of the outer sheath.

[0131] Alternatively or additionally, the imaging components may include an ultrasound transducer for ultrasound imagery, and/or a laser light input for spectroscopic imaging.

[0132] As discussed above, it is desirable for the instrument to be flexible in order to facilitate movement or rotation at the distal end during treatment. Movement or rotation can be achieved in any suitable manner. For example, one or more guide wires may be provided. Each guide wire may run longitudinally along the instrument and may be pulled at the proximal end in order to cause the distal end to move to one side. In an alternative embodiment, the outer sheath of the instrument may provide a guiding function. For example, one or more guide wires may be extruded into the wall of the outer sheath to allow for control of position of the distal end of the device.

[0133] The outer sheath may have a multi-layer or multi-component construction. As explained above, it may carry the coaxial cable, separate control wire(s), a fibre bundle (if provided separately, a communication cable for an image sensor (if provided), wires for a temperature sensor (if provided), etc. The outer sheath may comprise a multi-lumen catheter having a plurality of lumens for conveying these components independently. The outer sheath may be arranged to convey fluid e.g. to cool the coaxial cable and radiating tip. There may be an inflow lumen and outflow lumen to permit circulation of cooling fluid.

[0134] FIG. 11 is a schematic view of a bronchoscope 300 that is another embodiment of the invention. In this embodiment, the coaxial cable discussed above does not travel through the instrument channel of the scoping device. Instead, as discussed in more detail below, a coaxial transmission line structure is integrally formed in the instrument cord of the bronchoscope, e.g. around the instrument channel lumen.

[0135] The bronchoscope 300 illustrated in FIG. 11 comprises a body 302 having a number of input ports and an output port from which an instrument cord 304 extends. The instrument cord 304 comprises an outer jacket which surrounds a plurality of lumens. The plurality of lumens convey various things from the body 302 to a distal end of the instrument cord 304. One of the plurality of lumens is the instrument channel discussed above. Other lumens may include a channel for conveying optical radiation, e.g. to provide illumination at the distal end or to gather images from the distal end. The body 302 may include an eyepiece 308 for viewing the distal end. In order to provide illumination at the distal end, a light source 310 (e.g. LED or the like) may be connected to the body 302 by an illumination input port 311.

[0136] At the distal end of the instrument cord 304 a radiator 306 is mounted. The radiator 306 is arranged to receive microwave energy from a coaxial transmission line structure formed within the instrument cord 304 and emit a microwave field to ablate tissue present at the distal end. The radiator 306 can have a structure corresponding to any of the instruments discussed above with reference to FIGS. 2, 3, 4, 8A-8C, 9A-9B, and 10A-10C.

[0137] The body 302 includes a power input port 305 for connecting to a coaxial cable (e.g. a conventional coaxial cable) to transfer microwave energy from a suitable microwave generator (not shown) to the coaxial transmission line structure in the instrument cord 304.

[0138] As discussed above, it is desirable to be able to control the position of at least the distal end of the instrument cord 304. The body 302 may include a control actuator 312 that is mechanically coupled to the distal end of the instrument cord 304 by one or more control wires (not shown), which extend through the instrument cord 304. The control wires may travel within the instrument channel or within their own dedicated channels. The control actuator 312 may be a lever or rotatable knob.

[0139] FIG. 12 is a view down the axis of the instrument cord 304 to show how the coaxial transmission line structure is integrally formed.

[0140] In this embodiment there are four lumens within the instrument cord 304. The largest lumen is the instrument channel 314. In this embodiment, a coaxial transmission line structure 316 is formed in the wall of the instrument channel 314. The coaxial transmission line structure 316 comprises an inner conductive layer 318 that is separated from an outer conductive layer 320 by a layer of dielectric material 322. The thicknesses and materials for these layers are selected as known in the art to ensure that the coaxial transmission line structure 316 can convey microwave energy at relatively low loss. There may be a protective layer formed on the inner surface of the inner conductive layer 318.

[0141] The other lumens comprise a camera channel 324 and a pair of illumination channels 326, but the invention is not limited to this configuration. For example, there may be other lumens, e.g. for control wires or fluid delivery or suction.

[0142] Integrating the means for delivering microwave power into the instrument cord can provide a number of advantages. Firstly, it can enable larger diameter coaxial transmission line structures to be used within a given instrument cord diameter. This may enable the loss of the coaxial transmission line structure to be reduced, which in turn can enable higher power levels to be available at the distal end and/or less heating of the instrument cord during treatment. Secondly, it can free up the instrument channel for other uses. This may mean that the number of lumens and therefore the overall diameter of the instrument cord can be reduced. For example, the instrument channel may be arranged to convey fluid, e.g. for delivery into tissue at the distal end or for cooling the instrument cord during treatment.

[0143] FIG. 13 is a schematic cross-section view of a distal end of the instrument cord 304 described above, which shows one example of a connection to a radiator. In this example, the radiator comprises a coaxial cable 202 as discussed above. The same reference numbers are used for corresponding features, which are therefore not described again. In FIG. 13 only the proximal end of the coaxial cable 202 is shown. The distal end (not shown) can comprise a radiating tip 204 having the same form as those discussed above.

[0144] As shown in FIG. 13, the outer conductor 322 of the coaxial transmission line structure 316 is electrically connected to the outer conductor 208 of the coaxial cable 202 by a first radial conductive element 328, and the inner conductor 318 of the coaxial transmission line structure 316

is electrically connected to the inner conductor **206** of the coaxial cable **202** by a second radial conductive element **330**.

[0145] A pair of control wires **332** extend through the instrument channel **314** from the control actuator on the body, and are mounted within the outer sheath **218** of the coaxial cable **202**. As the coaxial cable is fixed to the distal end of the instrument cord **304**, relative longitudinal movement of the control wires **332** within the instrument channel **314** can cause the distal end of the coaxial cable **202** to move from side to side.

[0146] The embodiment shown in FIG. 13 shows how a control mechanism (i.e. a steering mechanism) for the radiator can be combined with an integrally formed power delivery configuration. In addition, this embodiment is an example where the power delivery structure is formed from a pair of coaxial transmission lines connected in series, where the outer diameter of the distal coaxial transmission line is less than the outer diameter of the proximal coaxial transmission line. Such a structure can provide an advantageous balance between the problem of power loss and the desire to have a physically small instrument to navigate the bronchial tree. The larger diameter proximal coaxial transmission line may be less lossy than the smaller diameter distal coaxial transmission line, so using this structure can enable power to be more efficiently delivered to a small instrument than would be the case if the same sized coaxial cable were used for the whole length of the instrument cord.

[0147] In the example shown in FIG. 13, the instrument channel **314** may be used to circulate fluid, e.g. for the purpose of cooling the coaxial transmission line **316** during treatment.

[0148] The distal coaxial cable **202** may be detachable from the instrument cord **304**. The structure shown in FIG. 12 may thus be usable with a variety of distal instrument configurations. Some examples are described below with reference to FIGS. 14 to 18. Features in common with FIG. 13 are given the same reference numbers and are not described again.

[0149] FIG. 14 shows an example in which an expandable balloon **334** is mounted at the distal end of the instrument channel. The balloon **334** may be inflated by the application of a suitable fluid through the instrument channel **314**, or may be manually operated using a control rod **336**, which can be connected to the inner surface of the balloon **334** by a plurality of connecting strands **338**. In one example, the balloon **334** may expand using fluid and may be retracted by pulling back on the control rod **336**.

[0150] The balloon **334** may be made from a flexible dielectric material which can act as a substrate for one or more radiating elements (not shown). The balloon may resemble an aortic balloon. The radiating elements may be patch antennas or the like, which are in electrical communication with the coaxial transmission line structure **316**.

[0151] FIG. 15 shows an example in which a radially expandable radiating structure **340** is mounted at the distal end of the instrument channel **314**. The radiating structure **340** may be tubular with a series of longitudinal slits in its outer surface. When a movable distal end **343** of the radiating structure **340** is brought towards a fixed proximal end **345**, the parts of the structure between the slits flares out radially. One or more radiating elements **346**, e.g. patch antennas or the like, may be mounted on the parts which

flare out. The radiating elements are in electrical communication with the coaxial transmission line structure.

[0152] The movable distal end **343** may be connected to a control rod **342** that is mounted in the instrument channel, e.g. via a pair of connector strands **344**.

[0153] FIG. 16 shows an example in which a forceps structure **350** is attached at the distal end of the instrument channel **314**. The forceps structure **350** comprises a pair of jaws **351** connected at a pivot point **353**. The pair of jaws **351** are capable of being opened and closed under operation of a control rod **352**, which may be mounted in a fixed sleeve **354** that extends through the instrument channel **314**.

[0154] One or both of the pair of jaws **351** has a radiating element **356** (e.g. patch antenna or the like) formed thereon, e.g. at an inner surface thereof. The radiating element **356** is in electrical communication with the coaxial transmission line structure **316**. In this example, the forceps structure **350** may be secured in the instrument channel **314** by a distal cap **362**. The distal cap **362** may include a pair of radial conductive elements **358**, **360** for providing electrical connections between the radiating element **351** and the inner conductor **318** and outer conductor **322** respectively of the coaxial transmission line structure **316**.

[0155] The forceps structure **350** can be used to grasp tissue in the bronchial tree.

[0156] FIG. 17 shows an example in which a paddle structure **364** is attached at the distal end of the instrument channel. Feature in common with FIG. 16 are given the same reference number and are not described again. The paddle structure **364** comprises a dielectric body **366** with one or more radiating elements **368** (e.g. patch antennas or the like) fabricated thereon. The radiating elements are electrically connected to the coaxial transmission line structure, e.g. via the radial conductive elements **358**, **360**. The position of the paddle may be controlled using a control rod **370**.

[0157] FIG. 18 shows a schematic distal tip portion **372** that incorporates temperature sensors **374** (e.g. thermocouples). The distal tip portion comprises a coaxial cable that can extend through the instrument channel of a bronchoscope or which can be connected at the distal end of a hollow coaxial transmission line structure that is integrated within the instrument cord, as discussed above.

[0158] In detail, the top portion **372** comprises a coaxial cable **376** comprising an inner conductor **378** separated from an outer conductor **380** by a first dielectric material **382**. The coaxial cable may be the same as the coaxial cable **202** discussed above. The coaxial cable **376** is encased in an outer jacket **384**, which has a plurality of temperature sensors **374** mounted therein. Signal lines **386** for the temperature sensors are also carried in the outer jacket **384**. The signal lines **386** extend proximally out of the instrument to provide information from the temperature sensors to an external monitoring device (not shown).

[0159] At the distal end of the coaxial cable **376** there is a radiating tip section **388** that comprises a distal conductive section **390** of the inner conductor **378** that extends beyond a distal end **392** of the outer conductor **380**. The distal conductive section **390** is surrounded at its distal end by a dielectric tip **394** formed from a second dielectric material, which is different from the first dielectric material **382**. The length of the dielectric tip **394** is shorter than the length of the distal conductive section **390**. An intermediate dielectric sleeve **396** surrounds the distal conductive section **390** between the distal end of the coaxial cable **376** and the

proximal end of the dielectric tip **394**. The intermediate dielectric sleeve **396** is formed from a third dielectric material, which is different from the second dielectric material but which may be the same as the first dielectric material **382**.

[0160] The radiating tip section **388** acts in the same manner as described above with respect to FIG. 3 in that it reduces the wavelength of the microwave energy to provide a more focussed field. Indeed, the radiating tip section may be configured in the same way as shown in any of FIGS. 2, 3, 4, 8A-8C, 9A-9B, and 10A-10C.

[0161] A dielectric cap **398** formed of a fourth dielectric material, which is different from the second dielectric material but may be the same as the first or third dielectric material **382**, **396** is formed at the distal end of the dielectric tip **394**. Similarly to FIG. 3, the second dielectric material may be TiO₂ and the third dielectric material may be PTFE. The fourth dielectric material may also be PTFE. A temperature sensor **375** can be mounted in the dielectric cap **398**. Signal lines from the temperature sensor **375** in the dielectric cap **398** may pass through the dielectric tip **394**.

[0162] As the signal lines for the temperature sensors are so close to the transmission line that carries the microwave energy, it may be necessary to take action to avoid the microwave energy swamping a response signal from the temperature sensors. In one example, this can be done by delivering the microwave energy in a series of pulses and taking readings from the temperature sensors in the gaps between the pulses.

[0163] In another example, the response signals from the temperature sensors may be extracted by filtering out any noise due to the microwave energy. FIG. 19 shows an example of a suitable filtering arrangement **400** for a thermocouple **401**. The filter arrangement **400** comprises a pair of low pass filters **402** and an instrumentation amplifier **404** arranged to remove any common noise from signals V_{sig1} , V_{sig2} on the wire legs **404**, **406** of the thermocouple **401**.

[0164] In the arrangement shown in FIG. 19, the output signal V_{out} can be expressed as

$$V_{out} = (V_{sig1} - V_{sig2}) \frac{R_2}{R_1} \left(1 + \frac{2R_3}{R_G} \right)$$

[0165] FIG. 20 shows an example of a suitable low pass filter **402** for the filtering arrangement **400**. The low pass filter **402** comprises a plurality (preferably three) stubs **410** formed on each wire leg **404**, **406** of the thermocouple. The stubs **410** are separated by a multiple of a half wavelength of the microwave energy, and have a height equal to an odd multiple of a quarter wavelength of the microwave energy.

1-44. (canceled)

45. An electrosurgical instrument for delivering microwave energy into biological tissue, the electrosurgical instrument comprising:

- a coaxial cable for conveying microwave energy, the coaxial cable having an inner conductor, an outer conductor, and a first dielectric material separating the inner conductor and outer conductor;
- a radiating tip portion disposed at a distal end of the coaxial cable to receive the microwave energy from the coaxial cable; and
- an imaging element for conveying an imaging signal to permit visualisation of a distal end of the instrument,

wherein the radiating tip portion comprises:

- a dielectric tip formed from a second dielectric material that is different from the first dielectric material, and
- a distal conductive portion of the inner conductor, which extends longitudinally into the dielectric tip, wherein the second dielectric material has a dielectric constant greater than the first dielectric material, the geometry of the second dielectric material and its dielectric constant being selected such that an axial length of the dielectric tip corresponds to a fraction of a wavelength of the microwave energy when propagating in the dielectric tip, whereby the radiating tip portion is arranged as a quarter wave impedance transformer to match an input impedance to a tissue load impedance to radiate a localized microwave field for tissue ablation,

wherein the imaging element extends through the first dielectric material and radiating tip portion within the inner conductor and distal conductive portion.

46. An electrosurgical instrument according to claim **45**, wherein the outer diameter of the coaxial cable and radiating tip portion is equal to or less than 1.9 mm.

47. An electrosurgical instrument according to claim **45**, wherein the dielectric constant of the second dielectric material is equal to or greater than 80.

48. An electrosurgical instrument according to claim **45**, wherein the radiating tip portion further comprises an intermediate dielectric element surrounding a proximal part of the distal conductive portion and separating the first dielectric material from the dielectric tip, the intermediate dielectric element being formed from a third dielectric material that is different from the second dielectric material.

49. An electrosurgical instrument according to claim **45**, comprising conductive material arranged on an outer surface of the dielectric tip to form a microstrip or coplanar transmission line for delivering the microwave energy into biological tissue.

50. An electrosurgical instrument according to claim **45**, wherein the radiating tip portion includes a field shaping element arranged to direct the microwave field to one side of the radiating tip portion.

51. An electrosurgical instrument according to claim **50**, wherein the field shaping element is a conductive finger extending longitudinally along a side of an outer surface of the dielectric tip opposite to the side from which the microwave field is directed, the conductive finger being electrically connected to the outer conductor of the coaxial cable.

52. An electrosurgical instrument according to claim **51**, wherein the radiating tip portion includes a dielectric cap disposed distally to the dielectric tip and distal conductive portion, the conductive finger extending along an outer surface of the dielectric cap, whereby the conductive finger extends further from the coaxial cable than the distal conductive portion.

53. An electrosurgical instrument according to claim **51**, wherein the conductive finger is an extension of the outer conductor of the coaxial cable.

54. An electrosurgical instrument according to claim **51**, wherein the conductive finger is a distal part of a conductive sleeve mounted on and electrically connected to the outer conductor of the coaxial cable, wherein the conductive sleeve is rotatable relative the dielectric tip to adjust the circumferential position of the conductive finger.

55. An electrosurgical instrument according to claim 50, wherein the field shaping element is a conductive sleeve formed over the dielectric tip, the conductive sleeve having a radiating slot formed therein on the side from which the microwave field is directed.

56. An electrosurgical instrument according to claim 55, wherein the conductive sleeve is rotatable relative the dielectric tip to adjust the circumferential position of the radiating slot.

57. An electrosurgical instrument according to claim 54, wherein the conductive sleeve has a pair of radiating slots on opposite sides of the dielectric tip, and wherein the radiating top portion comprises an actuator operable to selectively expose only one of the pair of radiating slots.

58. An electrosurgical instrument according to claim 57, wherein the actuator comprises a longitudinally slidable sleeve having opposed cut outs formed therein, wherein the actuator is movable between a first position in which a first cut out exposes a first one of the pair of radiating slots and a second position in which a second cut out exposes a second one of the pair of radiating slots.

59. An electrosurgical instrument according to claim 45, wherein the imaging element includes a fibroscope comprising a bundle of optical fibres.

60. An electrosurgical instrument according to claim 59, wherein the inner conductor and distal conductive portion are hollow to define a channel for carrying the bundle of optical fibres.

61. An electrosurgical instrument according to claim 59, wherein the bundle of optical fibres extends through the first dielectric material and radiating tip portion and has a layer of conductive material over its outer surface to form the inner conductor of the coaxial cable and the distal conductive portion.

62. An electrosurgical instrument according to claim 45, wherein the imaging element comprises an image sensor mounted at the distal end of the radiating tip portion and a communication cable for conveying a signal from the image sensor to the proximal end of the instrument.

63. An electrosurgical instrument according to claim 62, wherein the inner conductor and distal conductive portion are hollow to define a channel for carrying the communication cable.

64. An electrosurgical instrument according to claim 62, wherein the image sensor comprises an ultrasound transducer.

65. An electrosurgical instrument according to claim 45 including a temperature sensor at the distal end thereof.

66. An electrosurgical instrument according to claim 65, wherein the temperature sensor is a thermocouple mounted on the outer conductor of the coaxial cable.

67. An electrosurgical instrument according to claim 66, wherein the thermocouple comprises a plurality of stubs arranged to filter out a signal having the same frequency as the microwave energy.

68. An electrosurgical instrument according to claim 65, wherein the temperature sensor includes a temperature sensitive micromechanical structure at the distal end of the end, and a means of optically monitoring the temperature sensitive micromechanical structure.

69. An electrosurgical instrument according to claim 45, wherein the coaxial cable is mounted in an outer sheath, and wherein the outer sheath is a multi lumen catheter arranged to convey any one or more of:

guide wires for controlling movement of the radiating tip section, and fluid for cooling the distal end of the instrument.

70. An electrosurgical apparatus for delivering microwave energy into lung tissue, the electrosurgical apparatus comprising:

a generator for generating microwave energy;

a bronchoscope for non-percutaneous insertion into a patient's lungs, the bronchoscope having an instrument channel running along its length; and

an electrosurgical instrument according to claim 45 mounted in the instrument channel of the bronchoscope,

wherein the coaxial cable is connected to receive microwave energy from the generator.

71. An electrosurgical apparatus according to claim 70, wherein the generator is arranged to deliver pulses of microwave energy in time with the breathing cycle of the patient.

* * * * *

专利名称(译)	用于输送微波能量的电外科探针		
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申请(专利权)人(译)	CREO医药有限		
当前申请(专利权)人(译)	CREO医药有限		
[标]发明人	HANCOCK CHRISTOPHER PAUL WHITE MALCOLM BURN PATRICK SHAH PALLAV HALES PHILIP		
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摘要(译)

一种用于微创手术技术的电外科器械，其提供能够精确消融组织的小规模局部微波场，例如微波场。在肺中，通过适当选择几何形状和材料用于其辐射远端尖端。该器械可以与支气管镜一起使用，该支气管镜具有在其器械线内形成的功率输送结构。视觉系统可以结合到能量输送结构中。该仪器包括用于将微波能量传送到辐射尖端部分的同轴电缆，该辐射尖端部分包括电介质尖端和在其中纵向延伸的远端导电部分。电介质尖端的介电常数大于同轴电缆内的介电材料。该装置的远端设计成便于将有效的微波能量输送到肺肿瘤组织以实现局部消融体积。

