



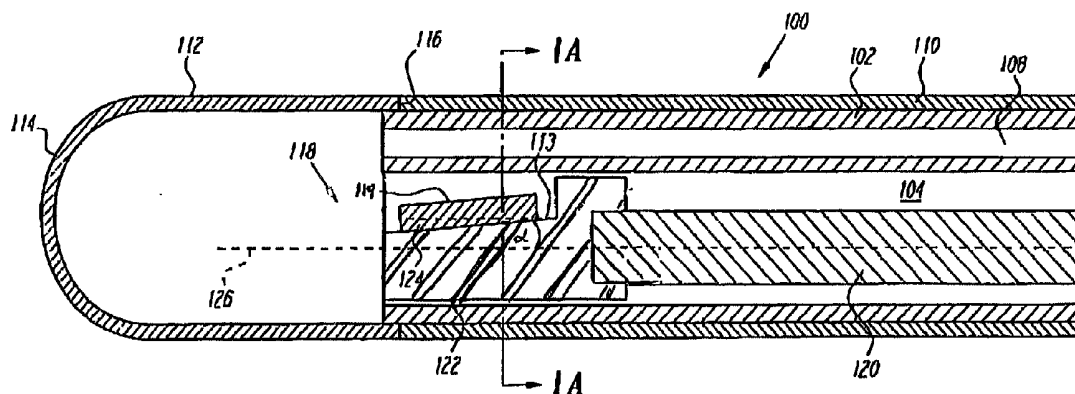
US 20040199047A1

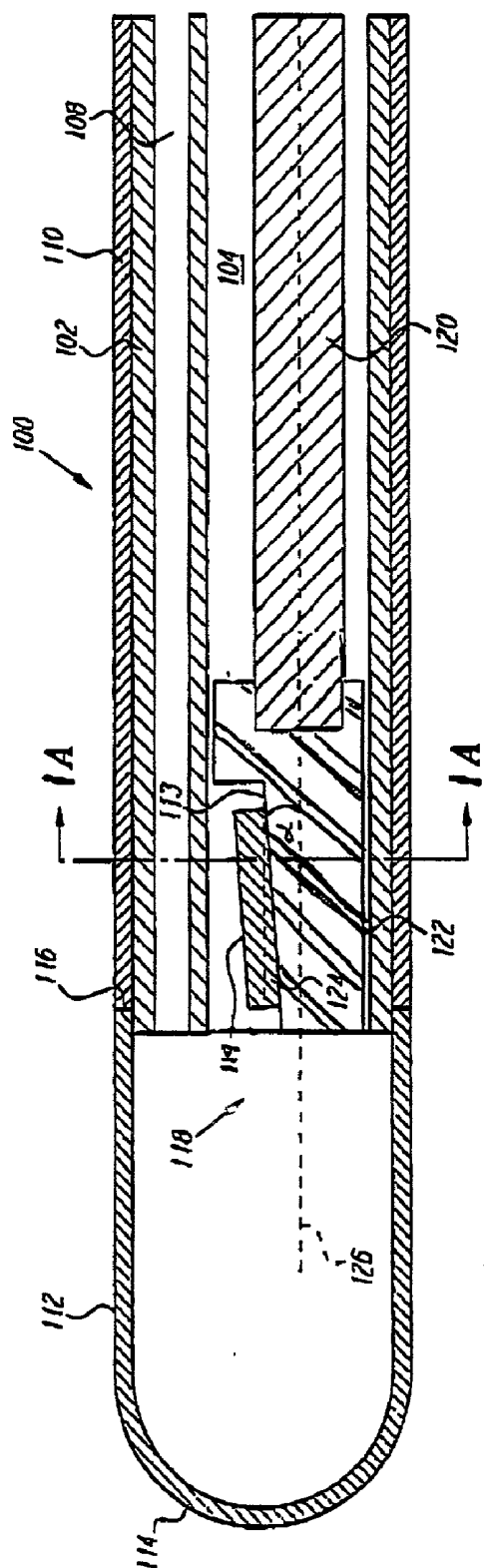
(19) **United States**(12) **Patent Application Publication**  
Taimisto et al.(10) **Pub. No.: US 2004/0199047 A1**(43) **Pub. Date: Oct. 7, 2004**(54) **TRANSDUCER WITH MULTIPLE  
RESONANT FREQUENCIES FOR AN  
IMAGING CATHETER****Publication Classification**(51) **Int. Cl.<sup>7</sup>** ..... A61B 1/00(52) **U.S. Cl.** ..... 600/101(76) **Inventors:** Mirian H. Taimisto, San Jose, CA  
(US); Richard Lardner, Oakland, CA  
(US)

Correspondence Address:

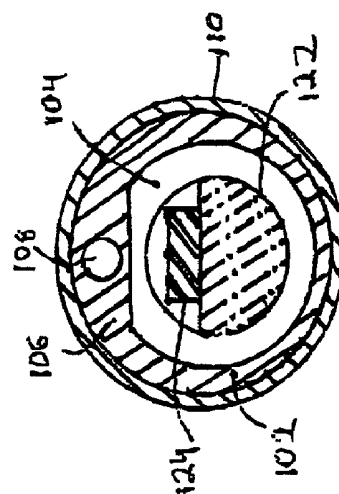
**ORRICK, HERRINGTON & SUTCLIFFE, LLP**  
**4 PARK PLAZA**  
**SUITE 1600**  
**IRVINE, CA 92614-2558 (US)**(21) **Appl. No.:** 10/167,223(22) **Filed:** Jun. 10, 2002(57) **ABSTRACT**

A single transducer element that is capable of oscillation at a plurality of natural resonant frequencies may be used in an ultrasonic imaging catheter assembly including a catheter body configured to be inserted and guided through the vascular system of a living being, a lumen and a rotatable imaging core adapted to pass through the lumen, the imaging core including a flexible drive-shaft. Because the transducer element is capable of oscillation at a plurality of natural resonant frequencies, a user can switch from one frequency to another in order to improve the depth of field or resolution without having to switch out the catheter or imaging core.





**FIG. 1**



**FIG. 1A**

## TRANSDUCER WITH MULTIPLE RESONANT FREQUENCIES FOR AN IMAGING CATHETER

### FIELD OF THE INVENTION

[0001] The present invention relates generally to the field of medical ultrasonic catheters, and in particular, to a transducer element having multiple resonant frequencies for use in ultrasonic imaging medical catheters.

### BACKGROUND OF THE INVENTION

[0002] In recent years, the use of ultrasound systems for medical diagnostics has continued to grow. Ultrasonic systems are used in a vast array of medical fields and diagnostic areas. As the desire to use ultrasonic imaging systems has grown, so has the level of sophistication of those systems.

[0003] To assist physicians and staff in performing diagnostic and therapeutic procedures, a number of ultrasonic imaging systems have been designed for use with catheters. In general, these systems comprise a single transducer element, frequently made of piezoelectric material, attached to the distal portion of an imaging catheter. The imaging catheter is inserted into the patient so that the transducer is positioned to image a desired region of the patient's anatomy.

[0004] Such catheters typically operate by sending an electrical signal or excitation pulse to the transducer. The transducer then converts the electrical energy into mechanical energy, which propagates into a patient's surrounding body tissues as ultrasonic waves. The frequency of the emitted ultrasonic waves are a function of the resonant frequency of the transducer element and the frequency content of the excitation pulse. The ultrasonic waves are reflected back to the transducer as reflected signals or echoes, which the transducer converts into an electrical signal, which is used to produce an image of the patient's anatomy.

[0005] By operating with a transducer having only one resonant frequency, however, the focusing capability of the imaging catheters is limited. The frequency of emitted sound waves is a function of the resonant frequency and bandwidth of the transducer element and the frequency content of the excitation pulse, and can only be altered by varying the excitation pulse frequency. As a result, the ability of the single resonant frequency transducer element to be focused at different depths into the surrounding tissue is limited.

[0006] Other catheter systems attempt to solve the focusing problem by switching out the catheter or imaging core during operation so that the replacement catheter would contain a transducer element with a different frequency. However, this method of catheter replacement is very time-consuming which necessarily makes the imaging procedure longer than is necessary.

[0007] Therefore, there exists a present need to provide a multiple resonant frequency transducer for an imaging catheter system, which is capable of providing high quality ultrasound images at different depths without having to switch out the catheter or the imaging core.

### SUMMARY OF THE INVENTION

[0008] A first, separate aspect of the invention involves an ultrasonic imaging catheter assembly including a catheter

body configured to be inserted and guided through the vascular system of a living being, the catheter body having a distal end, a proximal end, and a lumen extending through its longitudinal axis. The ultrasonic imaging catheter assembly further includes a rotatable imaging core adapted to pass through the lumen, the imaging core including a flexible drive-shaft and a single transducer element that is capable of oscillation at a plurality of natural resonant frequencies.

[0009] A second, separate aspect of the invention involves an ultrasonic imaging catheter assembly including a transducer having a plurality of natural resonant frequencies including a lower resonant frequency and a higher resonant frequency. During use in the vascular system of a living body, the transducer can be switched between the lower resonant frequency and the higher resonant frequency, wherein the transducer element is to be oscillated at the lower resonant frequency to optimize depth of penetration and wherein the transducer element is to be oscillated at the higher resonant frequency to optimize resolution. Switching between resonant frequencies is accomplished using, for example, an external instrument console and, consequently, does not require removal of the catheter body or imaging core from the vascular system of the living body.

[0010] A third, separate aspect of the invention involves an ultrasonic imaging catheter assembly including a transducer having a plurality of natural resonant frequencies including a lower resonant frequency, a middle frequency and a higher resonant frequency, wherein for example, the lower frequency is about 7.5 MHz, the middle frequency is about 10 MHz and the higher frequency is about 30 MHz. During use within the vascular system of a living being, the different frequencies can be used for different purposes. For instance, the lower frequency may be adapted for imaging within arteries, the middle frequency may be adapted for guiding the catheter into place and the higher frequency may be adapted for imaging within the heart.

[0011] A fourth, separate aspect of the invention involves an ultrasonic imaging catheter assembly including a generally disk-shaped cylindrical transducer formed from piezoelectric ceramic materials, piezocomposite materials, piezoelectric plastics, barium titanates, lead zirconate titanates, lead metaniobates, or polyvinylidene fluorides. The transducer is attached to the drive-shaft by a transducer housing, wherein the transducer may be mounted in a cut-away portion of the transducer housing such that it slopes at an angle with respect to the central axis of the drive-shaft to reduce internal reflections inside the catheter.

[0012] The invention may include any one of these separate aspects individually, or any combination of these separate aspects.

[0013] Other features and advantages of the invention will be evident from reading the following detailed description, which is intended to illustrate, but not limit, the invention.

### BRIEF DESCRIPTION OF THE DRAWINGS

[0014] The drawings illustrate the design and utility of preferred embodiments of the invention, in which similar elements are referred to by common reference numerals.

[0015] FIG. 1 is a cut-away partial side view of an ultrasound catheter assembly.

[0016] FIG. 1A is a cross-sectional view of the ultrasound catheter assembly of FIG. 1 taken along line 1A-1A.

#### DESCRIPTION OF THE PREFERRED EMBODIMENT

[0017] The improved transducer element having multiple resonant frequencies may be used, for example, in an ultrasound imaging system. Mechanical scanning ultrasound imaging catheter systems typically employ a single transducer mounted inside a rotating housing. In one example, the transducer transmits and receives ultrasonic waves while the transducer housing rotates about a fixed axis in an acoustic window located at a distal tip of the catheter. The rotational motion of the transducer housing is accomplished by a flexible drive-shaft that extends through an axially disposed lumen of the catheter, wherein the drive-shaft has one end connected to the transducer housing. Once the distal end of the catheter is positioned, for example, in a patient's vascular system, a cross-sectional image of the tissue surrounding the distal catheter tip is produced by using imaging and control circuitry that are electrically coupled to the transducer via an electrical conductor extending through the drive shaft.

[0018] FIGS. 1 and 1A illustrate an example embodiment of a flexible ultrasound catheter 100. Ultrasound catheter 100 is adapted to be positioned within the vascular system by standard, well-known catheter procedures by guiding the flexible catheter 100 through various blood vessels along a circuitous path, beginning, for example, by percutaneous introduction through a perforation of the femoral artery.

[0019] The catheter includes an elongate tubular member 102, which forms an axially disposed lumen 104. The inner dimensions of lumen 104 are sufficient to allow an imaging core 118 to be slidably disposed therein. The imaging core includes a flexible drive-shaft 120 connected to a transducer housing 122 having a generally disk-shaped transducer 124 mounted therein. The imaging core 118 is capable of translation along its central axis. In addition, imaging core 118 is capable of rotation about its central axis at speeds in excess of 1800 rpm. Further disclosure concerning rotatable, motor-driven imaging cores can be found in U.S. Pat. No. 6,004, 269, which is incorporated herein by reference.

[0020] A dome-shaped acoustic imaging window 112 is attached to a distal end of the elongate tubular element 102, thereby forming an enclosed tip of the catheter 100. Alternatively, the shape of the acoustic imaging window 112, the transducer 124, or any other component may be virtually any shape or combination of shapes. A cover tube 110 formed of a suitable material, such as a heat shrinkable nylon, urethane, polyethylene or other plastic, is disposed around tubular element 102, wherein cover tube 110 provides both structural integrity to the catheter 100, as well as a smooth outer surface for ease in axial movement in a patient's body passage with minimal friction.

[0021] Preferably, the acoustic imaging window 112 has its proximal end open and its distal end rounded and is attached to a distal outer circumferential portion of the tubular element 102 to form an enclosed catheter tip 114, with respective ends of the cover tube 110 and acoustic imaging window 112 bonded together at a common joint 116. The outer diameter of the proximal end of window 112 is substantially equal to that of the installed cover tube 110,

so that a smooth outer surface is provided at joint 116. As best seen in FIG. 1, optional upper portion 106 of the elongate tubular member 102 forms a smaller lumen 108, which can be used for other catheter functions such as, by way of non-limiting examples, housing pullwires, drug delivery, balloon angioplasty, laser ablation, or for housing a stiffening member to help prevent the collapsing of the catheter 100. Of course, the catheter may have any number of lumens of any configuration. The catheter could have a balloon or a plurality of balloons, if desired. The catheter could also have more than one window, wires embedded in the catheter walls, multiple transducers, or other features known in the field. For example, the catheter could use another transducer in addition to the multiple resonant frequency transducer. Optionally, the catheter could even use a plurality of multiple resonant frequency transducers.

[0022] With further reference to the particular example shown in FIG. 1, the transducer housing 122 has a longitudinally disposed cut-away portion 113, which slopes at a slight angle,  $\alpha$ , with respect to the central axis 126 of drive-shaft 120. The transducer 124 is mounted in the cut-away portion 113 of the transducer housing 122 such that its active surface 119 also slopes at angle  $\alpha$  with respect to central axis 126 of drive-shaft 120. This tilting of transducer 124 helps to minimize internal reflections inside of catheter tip 114.

[0023] Although the preferred transducer 124 of the present invention is disk-shaped, it may, alternatively, be any other shape. In use, it converts electrical energy pulses into mechanical energy, which propagates out from the face of the transducer 124 in the form of ultrasonic waves. The frequencies of these ultrasonic waves are dependent upon the excitation frequencies and the natural resonant frequencies of the transducer 124. The natural resonant frequencies of the transducer 124 are a product of the shape and thickness of the transducer 123 and the transducer material.

[0024] Transducer 124 is formed in a known manner from materials capable of transforming pressure distortions on its surface into electrical voltages and vice versa. Such materials include, but are not limited to piezoelectric ceramic materials, piezocomposite materials, piezoelectric plastics, barium titanates, lead zirconate titanates, lead metaniobates and polyvinylidene fluorides.

[0025] As discussed above, the frequency at which the transducer 124 emits ultrasonic waves is a function of the resonant frequencies of the transducer 124 and the frequency of the excitation pulse sent to the transducer 124. When the ultrasonic waves impinge on an object, the ultrasonic waves are reflected back to the transducer 124, which converts the mechanical energy back into an electrical signal. The electrical signal from the transducer 124 is transmitted from the distal end of the catheter 100 to the catheter system's imaging equipment by a transmission line.

[0026] By using an imaging catheter 100 with a transducer 124 having multiple resonant frequencies, a user is capable of producing images having varying characteristics depending upon which frequency is utilized. Two important imaging characteristics are depth of field and resolution. Depth of field permits greater penetration during operation, which can be useful for imaging the in the heart, for example. High resolution is important for close-up imaging within a vessel such as a coronary artery. However, good depth of field

comes at the expense of lower resolution and vice versa. Preferably, the improved transducer **124** is capable of operating at low, middle and high resonant frequencies in order to take advantage of the differing imaging characteristics of each frequency.

[0027] As an example, the multiple resonant frequency catheter **100** of the present invention can be configured to have three resonant frequencies at 30 MHz, 10 MHz and 7.5 MHz. In a single procedure, all three frequencies can be employed by a user. As an example, suppose an imaging procedure entails first imaging a coronary artery, then guiding the catheter **100** into the right atrium and then imaging the left atrium. To image the coronary artery, the transducer **124** should be operated at the 30 MHz frequency since the higher frequency yields good close-up resolution.

[0028] After imaging the coronary artery, the catheter must be guided into the right atrium. Since guiding the catheter into place requires both depth of field and resolution, the middle range frequency of 10 MHz is preferred for this maneuver. Upon guiding the catheter into place in the right atrium, the left atrium is to be imaged. Imaging the atrium at a distance will require considerable depth of field and the lower 7.5 MHz resonant frequency will, therefore, be preferable at this stage. In this manner, all three resonant frequencies can be employed in a typical imaging procedure. However, this procedure is merely one example of a myriad of imaging procedures that require a transducer to operate at multiple frequencies.

[0029] Because the multiple resonant frequency transducer **124** is capable of oscillation at three resonant frequencies, the catheter and/or imaging core does not have to be switched out during operation. Switching catheters out is a timely procedure, which necessarily makes the imaging procedure longer than is necessary. Instead, a catheter can use a single transducer **124** having multiple resonant frequencies, without having to sacrifice depth of field or resolution. Switching between resonant frequencies may be accomplished, for example, using an external instrument console. Any number of typical instrument console expedients can be used to accomplish this task including a button, dial, switch, voice command, mouse, track ball, or pointing device.

[0030] Any one or more of the features depicted in **FIGS. 1 and 1A**, or described in the accompanying text, may be interchanged with that of another figure to form still other embodiments.

[0031] While preferred embodiments and methods have been shown and described, it will be apparent to one of ordinary skill in the art that numerous alterations may be made without departing from the spirit or scope of the invention. Therefore, the invention is not limited except in accordance with the following claims.

What is claimed is:

1. An ultrasonic imaging catheter assembly comprising;

a catheter body configured to be inserted and guided through the tissues of a living being, the catheter body having a distal end, a proximal end, and a lumen extending through its longitudinal axis; and

a rotatable imaging core adapted to pass through the lumen, the imaging core including a flexible drive-shaft and a transducer element;

wherein the transducer element is capable of oscillation at a plurality of natural resonant frequencies.

2. The ultrasonic imaging catheter assembly of claim 1, wherein the plurality of natural resonant frequencies includes a lower resonant frequency and a higher resonant frequency.

3. The ultrasonic imaging catheter assembly of claim 2, wherein the transducer element is switchable between a lower resonant frequency and a higher resonant frequency during use of the catheter assembly within tissue.

4. The ultrasonic imaging catheter assembly of claim 3, wherein the transducer element is switchable to oscillate at the lower resonant frequency to increase the depth of penetration within the tissue.

5. The ultrasonic imaging catheter assembly of claim 3, wherein the transducer element is switchable to oscillate at the higher resonant frequency to increase resolution within the tissue.

6. The ultrasonic imaging catheter assembly of claim 3, wherein switching between resonant frequencies does not require removal of the catheter body or imaging core from the tissue.

7. The ultrasonic imaging catheter assembly of claim 3, wherein switching between frequencies is accomplished using an external instrument console.

8. The ultrasonic imaging catheter assembly of claim 2, further including a middle resonant frequency.

9. The ultrasonic imaging catheter assembly of claim 1, further comprising a generally cylindrical acoustic imaging window at the distal tip of the catheter body.

10. The ultrasonic imaging catheter assembly of claim 1, wherein the transducer has a generally circular surface.

11. The ultrasonic imaging catheter assembly of claim 10 wherein the transducer is a disk-shaped cylinder.

12. The ultrasonic imaging catheter assembly of claim 1, wherein the catheter body further includes a second lumen.

13. The ultrasonic imaging catheter assembly of claim 12, wherein the second lumen is adapted to house a steering pullwire.

14. The ultrasonic imaging catheter assembly of claim 1, wherein the imaging core further includes a transducer housing that attaches the transducer to the drive-shaft.

15. The ultrasonic imaging catheter assembly of claim 14, wherein the transducer housing has a cut-away portion which slopes at an angle with respect to the central axis of the drive-shaft.

16. The ultrasonic imaging catheter assembly of claim 15, wherein the transducer is mounted in the cut-away portion such that it slopes at an angle with respect to the central axis of the drive-shaft.

17. The ultrasonic imaging catheter assembly of claim, wherein the transducer is formed from a piezoelectric ceramic material, piezocomposite material, piezoelectric plastic, barium titanate, lead zirconate titanate, lead metaniobate, or polyvinylidene fluorides.

18. The ultrasonic imaging catheter assembly of claim 1, wherein the plurality of natural resonant frequencies comprises three resonant frequencies including a higher, lower and middle frequencies.

19. The ultrasonic imaging catheter assembly of claim 18, wherein the higher resonant frequency is adapted for imaging within a heart of the living being.

20. The ultrasonic imaging catheter assembly of claim 19 wherein the higher resonant frequency is about 30 MHz.

21. The ultrasonic imaging catheter assembly of claim 18, wherein the lower resonant frequency is adapted for imaging within an artery of the living being.

22. The ultrasonic imaging catheter assembly of claim 21 wherein the lower resonant frequency is about 7.5 MHz.

23. The ultrasonic imaging catheter assembly of claim 18, wherein the middle resonant frequency is adapted for guiding the catheter body into place within the tissues of the living being.

24. The ultrasonic imaging catheter assembly of claim 23 wherein the middle resonant frequency is about 10 MHz.

25. The ultrasonic imaging catheter assembly of claim 19, wherein the lower resonant frequency is adapted for imaging within an artery of the living being.

26. The ultrasonic imaging catheter assembly of claim 25, wherein the middle resonant frequency is adapted for guiding the catheter body into place within the tissues of the living being.

27. The ultrasonic imaging catheter assembly of claim 1, wherein the transducer element is the only transducer element in the catheter assembly.

28. The ultrasonic imaging catheter assembly of claim 1 further comprising a second transducer element.

29. The ultrasonic imaging catheter assembly of claim 28 wherein the second transducer element is also capable of oscillation at a plurality of natural resonant frequencies.

\* \* \* \* \*

|                |   |         |            |
|----------------|---|---------|------------|
| 专利名称(译)        | 具有多个共振频率的换能器用于成像导管                              |         |            |
| 公开(公告)号        | <a href="#">US20040199047A1</a>                 | 公开(公告)日 | 2004-10-07 |
| 申请号            | US10/167223                                     | 申请日     | 2002-06-10 |
| [标]申请(专利权)人(译) | TAIMISTO密里安^ h<br>拉德纳RICHARD                    |         |            |
| 申请(专利权)人(译)    | TAIMISTO密里安H.<br>拉德纳RICHARD                     |         |            |
| 当前申请(专利权)人(译)  | TAIMISTO密里安H.<br>拉德纳RICHARD                     |         |            |
| [标]发明人         | TAIMISTO MIRIAN H<br>LARDNER RICHARD            |         |            |
| 发明人            | TAIMISTO, MIRIAN H.<br>LARDNER, RICHARD         |         |            |
| IPC分类号         | A61B8/12 A61B1/00                               |         |            |
| CPC分类号         | A61B8/12 A61B8/445 A61B8/4461                   |         |            |
| 其他公开文献         | US7396332                                       |         |            |
| 外部链接           | <a href="#">Espacenet</a> <a href="#">USPTO</a> |         |            |

#### 摘要(译)

能够以多个固有共振频率振荡的单个换能器元件可以用在超声成像导管组件中，该超声成像导管组件包括导管主体，该导管主体被配置成插入并引导通过生物的血管系统，内腔和可旋转成像。核心适于穿过内腔，成像核心包括柔性驱动轴。因为换能器元件能够以多个固有共振频率振荡，所以用户可以从一个频率切换到另一个频率，以便在不切换导管或成像核心的情况下改善景深或分辨率。

