



(11) **EP 1 272 110 B1**

(12) **EUROPEAN PATENT SPECIFICATION**

(45) Date of publication and mention
of the grant of the patent:
04.05.2011 Bulletin 2011/18

(21) Application number: **01926502.4**

(22) Date of filing: **30.03.2001**

(51) Int Cl.:
A61B 17/22 (2006.01)

(86) International application number:
PCT/US2001/010357

(87) International publication number:
WO 2001/074255 (11.10.2001 Gazette 2001/41)

(54) **EXPANSIBLE SHEARING CATHETERS FOR THROMBUS AND OCCLUSIVE MATERIAL
REMOVAL**

AUSWEITBARE SCHERKATHETER ZUR ENTFERNUNG VON THROMBUS UND
VERSCHLIESSENDEM MATERIAL

CATHETERS CISAILLANTS DILATABLES D'ELIMINATION DES THROMBUS ET DES
SUBSTANCES OBSTRUANTES

(84) Designated Contracting States:
**AT BE CH CY DE DK ES FI FR GB GR IE IT LI LU
MC NL PT SE TR**

(30) Priority: **31.03.2000 US 193539 P**
04.01.2001 US 260170 P
27.03.2001 US 820301

(43) Date of publication of application:
08.01.2003 Bulletin 2003/02

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WO-A-99/16365 WO-A2-99/56801
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Description

BACKGROUND OF THE INVENTION

1. Field of the Invention

[0001] The present invention relates generally to medical devices and methods. In one embodiment, the present invention relates to devices and methods for disrupting, collecting, and removing thrombus and/or other occlusive material from blood vessels.

[0002] Thrombosis and atherosclerosis are common ailments which occur in humans and which result from the deposition of thrombus and clot on the walls of blood vessels. When hardened, such deposits are commonly referred to as plaque. Such deposits are most common in the peripheral blood vessels that feed the limbs of the human body and the coronary arteries which feed the heart. Stasis, incompetent valves, and trauma in the venous circulation cause thrombosis, particularly occurring as a deep vein thrombosis in the peripheral vasculature. When such deposits build-up in localized regions of the blood vessel, they can restrict blood flow and cause a serious health risk.

[0003] In addition to forming in the natural vasculature, thrombosis is a serious problem in "artificial" blood vessels, particularly in peripheral femoral-popliteal and coronary bypass grafts and dialysis access grafts and fistulas. The creation of such artificial blood vessels generally involves anastomotic attachment at at least one, and usually at at least two, locations in the vasculature. Such sites of an anastomotic attachment are particularly susceptible to thrombus formation due to narrowing caused by intimal hyperplasia, and thrombus formation at these sites is a frequent cause of failure of the implanted graft or fistula. The arteriovenous grafts and fistulas which are used for dialysis access are significantly compromised by thrombosis at the sites of anastomotic attachment and elsewhere. Thrombosis often occurs to such an extent that the graft needs to be replaced within a few years or, in the worst cases, a few months.

[0004] A variety of methods have been developed for treating thrombosis and atherosclerosis in the coronary and peripheral vasculature as well as in implanted grafts and fistulas. Such techniques include surgical procedures, such as coronary artery bypass grafting, and minimally invasive procedures, such as angioplasty, atherectomy, transmyocardial revascularization, and the like. In many of the surgical clinical approaches to removing unwanted material, the treatment site is accessed directly through a surgical incision. Of particular interest of the present invention, a variety of techniques generally described as "thrombectomy" have been developed. Thrombectomy generally refers to procedures for the removal of relatively soft thrombus and clot from the vasculature. Removal is usually achieved by mechanically disrupting the clot, optionally with the introduction of thrombolytic agents. The disrupted thrombus or

clot is then withdrawn through a catheter, typically with a vacuum or mechanical transport device.

[0005] Thrombectomy generally differs from angioplasty and atherectomy in the type of occlusive material which is being treated and in the desire to avoid damage to the blood vessel wall. The material removed in most thrombectomy procedures is relatively soft, such as the clot formed in deep vein thrombosis, and is usually not hardened plaque of the type treated by angioplasty in the coronary vasculature. Moreover, it is usually an objective of thrombectomy procedures to have minimum or no deleterious interaction with the blood vessel wall. Ideally, the clot will be disrupted and pulled away from the blood vessel wall with no harmful effect on the wall itself.

[0006] While successful thrombectomy procedures have been achieved, most have required comprise between complete removal of the thrombosis and minimum injury to the blood vessel wall. While more aggressive thrombectomy procedures employing rotating blades can be very effective at thrombus removal, they can present a significant risk of injury to the blood vessel wall. Alternatively, those which rely primarily on vacuum extraction together with minimum disruption of the thrombus, often fail to achieve sufficient thrombus removal.

[0007] In work related to the present invention, an expansible macerator for safely breaking up or disrupting thrombus and other occlusive materials has been proposed. U.S. Patent 6454775 filed on December 6, 1999 and entitled "Systems and Methods for Clot Disruption and Retrieval," describes a catheter having an expansible positioning cage and a helical macerator positioned within the cage. The macerator can be separated from the surrounding cage so as to maintain separation between the macerator and a surrounding wall of the body lumen. This caged macerator represents a significant advancement in the art, as it allows disruption of soft clot while inhibiting trauma to blood vessels of varying diameters. However, as with all advances, still further improvements would be desirable. In particular, it may be beneficial to provide more aggressive and more rapid removal of clot material. It would also be helpful to allow the physician to selectively and controllably remove plaque or other more solid occlusive material during a thrombectomy, preferably using the thrombectomy catheter. It may also be beneficial to more uniformly urge the severed debris toward an aspiration port of the thrombectomy catheter. Finally, it may also be beneficial to find additional beneficial uses for similar and/or related catheter structures.

[0008] As mentioned, atherectomy has been proposed for treatment of the hardened plaque of atherosclerosis. Atherectomy may also remove occlusive tissues proliferating from the vessel wall. While a variety of atherectomy structures and devices have been proposed, and although a variety of atherectomy structures have been made commercially available on the market, the efficacy and use of atherectomy has remained somewhat limited, particularly when compared to alternative treatments for

stenotic disease.

[0009] Many of the vascular catheter devices recently developed for fragmentation and removal of plaque and/or thrombus, and for other intraluminal and intravascular procedures, are inserted percutaneously through a puncture in the skin. For example, a catheter device may be inserted into a blood vessel at some distance away from the intended treatment site, and can then be advanced through the vessel lumen until the selected location is reached. In most instances this approach is performed "over the wire," a technique in which the physician first places a guidewire device into the vessel lumen, so that the larger treatment catheter device can be tracked over the guidewire. In many cases the vessel to be treated is effectively blocked by an occlusive lesion (sometimes referred to as a "total occlusion," the occlusive lesion usually comprising, thrombus, soft plaque, and/or calcified plaque) so that advancing a guidewire to and/or beyond the lesion is challenging and/or impossible.

[0010] Several techniques and devices can assist in problematic intraluminal procedures, including guided or steerable guidewires and catheters, blunt-ended catheters, and the like. Once a guidewire or guiding catheter is placed, various techniques can be employed to fragment the unwanted plaque or tissue from blood vessels, including rotating abrasion structures or impeller, cutters, high pressure fluid infusion to create a Venturi effect, and the like. Other devices such as atherectomy cutters may also be employed. These known catheters and techniques for accessing and treating luminal lesions have had varying degrees of success. Unfortunately, total occlusions can impede access to the treatment site, making it challenging and/or impossible to place a guide structure for most of these subsequent treatments.

[0011] In light of the above, it would be beneficial to provide improved devices, systems, methods, methods for manufacture, and kits for removing occlusive material from the vasculature. It would be particularly desirable to provide improved techniques for advancing a guidewire or guide catheter, positioning a treatment catheter across the blocking occlusion, isolating the treatment site, and further treating the occlusion while minimizing or eliminating any distal emboli. An improved procedure would also benefit from having a device that can rapidly aspirate the occlusive material from the vasculature.

[0012] Optionally, these improved devices and methods might be used to treat a total occlusion as the treatment device is being advanced through the occlusion, facilitating placement of a wire across the occlusion so that further treatment can be easily commenced. Device and methods which allow creation of a channel through a total occlusion for placement of a guidewire would also be advantageous, as would improved debulking of stenotic tissues.

[0013] Some or all of these objectives may be met by the device of the present invention.

2. Description of the Background Art

[0014] As mentioned above, systems and methods for clot disruption and removal related to the present invention are described in U.S. Patent 6454775. A related mechanical pump for removal of fragmented matter and methods was described in U.S. Patent 6702830, filed on June 9, 2000. A further related method and system for reinfusing filtered body aspirates is described in PCT Application number WO 2001/49341, filed on December 28, 2000.

[0015] A cutting stent with a flexible tissue extractor is described in U.S. Patent No. 6,036,708. A compressible/expandable atherectomy cutter is described in U.S. Patent No. 5,224,945. Unitary removal of plaque is described in U.S. Patent No. 5,665,098. A method for performing a partial atherectomy is described in U.S. Patent No. 5,282,484, while an atherectomy device having a helical blade and a blade guide is described in U.S. Patent No. 5,569,277. A catheter arthrotome is described in U.S. Patent No. 5,178,625. A surgical apparatus for transurethral resection is described in U.S. Patent No. 3,320,957. A vessel deposit sharing apparatus is described in U.S. Patent No. 5,527,326.

[0016] A coiled stent with locking ends is described in U.S. Patent No. 5,725,549. A medical instrument with a slotted memory metal tube is described in U.S. Patent No. 5,885,258. A method for manufacturing a tubular medical device is described in U.S. Patent No. 6,027,863. The following U.S. Patent Nos. may also be relevant: 6,010,449; 5,968,064; 5,741,270; 5,766,191; 5,569,275; 5,501,694; 5,795,322; 5,904,968; 5,224,945; 5,312,425; 5,330,484; and 6,022,336.

[0017] US 3320957 discloses a transurethral resecting surgical instrument for use in performing prostatic surgical operations. The instrument includes inner and outer helical struts in which the inner struts may be rotated against the outer struts to shear off tissue that extends between the struts.

SUMMARY OF THE INVENTION

[0018] The present invention provides a vascular obstruction removal catheter, for removing thrombus and/or other obstructive material from the vasculature. The invention generally makes use of cooperating radially expandable shearing members, each shearing members often being in the form of an expandable basket. The exemplary baskets comprise helically oriented struts, with the struts of each shearing member extending with a uniform circumferential direction. The struts will often be independently flexible between proximal and distal portions of the shearing members, which can allow the shearing the members to flex axially to follow axially curving vasculature. The inner basket may be rotatably driven within the outer basket, and may optionally be coupled to an axial pump extending proximally from the shearing members. The outer basket may be coupled to a catheter

body to avoid excessive tissue trauma to the vasculature and the helical struts of the shearing members can be helically counterwound, so that the inner struts may slide substantially continuously across the outer struts. The inner and outer baskets may both radially expand selectively, independently and/or with a single actuator. The resulting shearing action is sufficiently aggressive for highly effective thrombectomy, while use of a rotationally static and axially flexible outer basket may provide a safe, limited, and controllable atherectomy treatment.

[0019] In a first aspect, the invention provides a vascular obstruction removal catheter comprising: a flexible tubular body having a proximal end and a distal end; an outer shearing member attached near the distal end, the outer member having a perforate inner surface; an inner shearing member rotatably disposed within the outer member, the inner member having a proximal portion, a distal portion, and a circumferential series of struts extending therebetween along a longitudinal axis of the inner shearing member, the struts sliding along the inner surface of the outer shearing member when the inner shearing member rotates; wherein the inner and outer shearing members are expansible between an unexpanded state and an expanded state, wherein the struts are helically oriented, and wherein in the unexpanded state a local pitch of the struts varies along the longitudinal axis of the inner shearing member.

[0020] Optionally, the inner member may rotate about an axis, and the inner and outer shearing bodies may be sufficiently flexible to deflect the axis laterally when the outer shearing member is expanded to engage a surrounding vessel and the inner member rotates therein. The struts may uniformly coil helically in a first circumferential orientation so that rotation of the inner shearing member toward the first circumferential orientation consistently urges sheared occlusive material proximally. The inner shearing member may comprise tube material, the struts being separated by cut surfaces between adjacent tube material portions. The outer shearing member may comprise outer tube material having a proximal outer portion, a distal outer portion and a circumferential series of outer struts extending helically therebetween, with the struts being separated by cut outer surfaces between outer adjacent tube material portions. The struts may be affixed together at the proximal portion and at the distal portion, and may flex independently therebetween.

[0021] The local pitch of the struts can increase toward the proximal and distal portions sufficiently to inhibit excessive separation between adjacent struts when the outer shearing member flexes axially. The struts may have protrusions which inhibit sliding of obstructive material axially between cooperating edges of the inner and outer shearing bodies. At least one expansion actuator may extend proximally from the shearing members so that the inner and outer shearing members can be radially expanded *in situ*. Axial translation of an expansion actuator may selectively radially expand the inner and outer

shearing members concurrently.

[0022] A distally oriented occlusion penetrator may be disposed adjacent the distal end of the shearing members. The occlusion penetrator may comprise one or more end cutters that rotate with the inner shearing member and are exposed distally of the outer shearing member to help advance the shearing members distally through occlusive material and within a vasculature. Alternative occlusion penetrators include a shaft extendable distally of the shearing members, the shaft axially oscillating through occlusive material without penetrating through a vessel wall. An intravascular ultrasound sensor can be used to measure vascular obstructions for removal and/or identify partial or total occlusion that may impede access to the target region.

[0023] It may also be desirable to attach a porous or non-porous coverings or coatings to at least one shearing member, particularly to the outer shearing member. Such a covering or coating may extend between the struts of a shearing member or positioning cage when the shearing member or positioning cage expands, and can be made from PTFE woven material, filter material (metallic or polymeric), braid material (metallic or polymeric), mesh, polymeric coatings, and the like. The coatings can be applied to the outer basket through a dipping process. Alternatively, the coverings may be applied to the outer basket using cyanoacrylate or other adhesives, thread or suturing, welding or bonding, or the like. Such coatings may be disposed along a distal and/or proximal region of the expandable perforate shearing member or positioning cage, and may inhibit embolization of fragmented occlusive material, constrain a treatment fluid or fluid stream, and the like.

[0024] In another aspect, the invention also provides a method for forming a vascular obstruction removal catheter, the method comprising: providing a first tube having a proximal end and a distal end with a central region therebetween, the tube comprising a tube material; cutting axially along the central region of the first tube so as to define a circumferential series of independent struts along a longitudinal axis of the first tube to define a first cage, the struts comprising the tube material; positioning the first cage coaxially with a second resiliently deformable cage; attaching a drive for rotating at least one of the cages within a blood vessel for shearing of obstructive material between the cages; wherein the cages are expansible between an unexpanded state and an expanded state, wherein the struts are helically oriented and wherein in the unexpanded state a local pitch of the struts varies along the longitudinal axis of the first tube.

[0025] In yet another aspect, the invention provides a component for use in a catheter device for removal of obstructive material from the lumen of a body conduit, said component comprising: first and second end portions having a longitudinal axis therebetween; a middle portion having at least one second cross sectional diameter and further comprising one or more flexible struts around the circumference of said longitudinal axis and

extending between, but not along, said first end portion and said second end portion; and wherein said middle portion and said end portions are formed from a continuous tube that is expansible between an unexpanded state and an expanded state, wherein the struts are arranged in a helical orientation and wherein in the unexpanded state a local pitch of the struts varies along said longitudinal axis.

[0026] The struts may have a width and a thickness, wherein said width is greater than said thickness. The width of the struts may vary along the length of the struts, and may form at least one serration or pocket. The thickness of the struts may be varied along the length of said strut, optionally so as to form a cutting edge. A cross section of the middle portion may be greater than cross sections of said end first and second end portions. The struts may be formed by laser cutting, by photoetching, by EDM, or by water jet abrasion. The first and second end portions can be formed in a zigzag configuration, and may have a longitudinal length that is less than that of the length of said middle portion. The component can comprise a shape memory alloy (such as a nickel titanium alloy, Elgiloy®, or the like), stainless steel, a formable polymer, a composite material, or the like.

BRIEF DESCRIPTION OF THE DRAWINGS

[0027]

Fig. 1 is a perspective view of inclusive material removal catheter having a rotationally driven inner basket which cooperates with a outer basket to shear occlusive material therebetween.

Fig. 2 is a perspective view of the distal portion of the catheter of Fig. 1.

Fig. 3A-3C is a perspective view showing the inner and outer baskets of the catheter of Fig.1. 3B and 3C show how the outer basket may have a coating or covering for embolic capture.

Fig. 4 is a perspective view of an outer basket or shearing member of the catheter of Fig. 1.

Fig. 5 is a perspective view of a tube cut so as to form the inner or outer basket of the catheter of Fig. 1.

Fig. 6 illustrates a flat pattern of the basket of Fig. 5, showing variable pitch of the helical struts.

Fig. 7 is a perspective view of an alternative basket having protrusions and/or circumferential indentations to inhibit axial sliding of occlusive material during shearing.

Fig. 8 is a perspective view of yet another alternative basket having circumferential proximal and/or distal web members between struts to inhibit severing of valves and other structures disposed axially of the shearing baskets.

Fig. 9 is a cross-sectional view of the connection between the proximal end of the shearing baskets and the distal end of the catheter body.

Fig. 10 is a simplified cross-sectional view of the

proximal end of the shearing baskets and the distal end of the catheter.

Fig. 11 is a cross-sectional view showing attachment of the inner shearing basket to a drive shaft.

Fig. 12 is a perspective view of a proximal housing of the catheter of Fig. 1.

Fig. 13 is a perspective view of the housing of Fig. 12 with a portion of the cover removed to show the drive system and other internal components.

Figs. 14-17 schematically illustrate the use of the occlusive material removal catheter of Fig. 1.

Figs. 18A and 18B illustrate alternative embodiments of the positioning cage catheter device of the present invention.

Figs. 18C-18F illustrate radially expandable positioning and shearing structures having an occlusive material penetrator in the form of a distally exposed morcellator for forming a passage through a total occlusion.

Fig. 19 illustrates the positioning cage catheter device of the present invention being used to initiate the crossing of a total occlusion.

Fig. 20 illustrates an alternative embodiment of the present invention wherein a positioning cage and a treatment device are formed integrally and placed over a guidewire.

Fig. 21 illustrates details of the distal end of the integral positioning cage and treatment device of Fig. 20.

Figs. 22, 23, and 24A-24B illustrates steps in methods for use of the system of Fig. 20 for accessing a treatment site of an occlusion which is challenging and/or impossible to traverse with a standard guidewire.

Fig. 25A-25C illustrates method of treating luminal occlusions in which a treatment region of the lumen is at least partially isolated.

Fig. 26 illustrates an alternative embodiment of the present invention wherein a drive shaft is advanced to gain access through the total occlusion.

DESCRIPTION OF THE SPECIFIC EMBODIMENTS

[0028] Referring now to Fig. 1, a vascular obstruction removal catheter 10 generally includes an elongate flexible catheter body 12 having a proximal end 14 and a distal end 16. Cooperating inner and outer shearing baskets 18, 20 define shearing means 19, and are disposed near distal end 16 of catheter body 12, while a proximal housing 22 is disposed near proximal end 14 of the catheter body. More specifically, outer basket 20 will typically be affixed at distal end 16 of catheter body 12, while a drive shaft drivingly couples inner basket 18 to a drive motor of proximal housing 22.

[0029] The inner and outer baskets 18, 20 of shearing means 19 are illustrated with some of the adjacent structures in Fig. 2, and in a simplified format (without some of the adjacent structures) in Fig. 3A. Outer basket 20 is

shown without inner basket 18 in Fig. 4.

[0030] Each of the baskets 18, 20 includes a proximal portion 24, a distal portion 26, and an intermediate portion 28. Intermediate portion 28 includes a circumferential series of helical struts 30. Struts 30 are affixed together at proximal portion 24 and distal portion 26, but generally extend independently therebetween. This allows struts 30 to flex individually, and allows the overall axis of each basket 18, 20 (as well as shearing means 19) to deflect laterally so as to accommodate axial curvature of the vasculature.

[0031] Baskets 18, 20 will generally be radially expandable *in situ* from a low profile configuration to a larger profile configuration. Baskets 18, 20 will often comprise a resilient or superelastic material, and may be biased to expand radially when released from a radially constraining sheath. As helically wound baskets exhibit radial expansion which is coupled with a decrease in axial length, manipulation of the axial lengths of the baskets may also be used to induce or control the radial expansion, so that baskets 18, 20 may expand resiliently when released from an axial elongation restraint.

[0032] The baskets may also be biased toward a profile which is smaller than a fully radially expanded configuration, so that radially and/or axial restraints are used to actively expand the diameter of shearing means 19. In other words, by decreasing the length of baskets 18, 20, struts 30 may be pushed radially outwardly. In the exemplary embodiment, inner and outer baskets 18, 20 will expand radially when an axial actuator 34 of proximal housing 22 (see Fig. 1) is actuated from outside the patient body, as will be described hereinbelow. Hence, struts 30 may optionally be biased toward the radially expanded configuration, a low-profile configuration, or some configuration therebetween. Advantageously, the profile of shearing means 19 can be selected from a plurality and/or continuous range of expanded sizes, and can be varied during treatment.

[0033] Outer basket 20 may be rotationally coupled to catheter body 12. Thus, movement of the outer basket within the vasculature can be substantially limited to, for example, axial positioning and advancement of the shearing means for treatment, thereby inhibiting excessive trauma to the surrounding vessel wall. Optionally, additional manipulation of catheter body 12 may be used to abraid the vessel wall with direct engagement between the outer basket and the endothelium.

[0034] Struts 30 of outer basket 20 have continuous inner surfaces 36 between proximal portion 24 and distal portion 26. Similarly, struts 30 of inner basket 18 may have continuous outer surfaces 38 between the proximal and distal portions. By rotationally driving inner basket 18 within outer basket 20 using drive shaft 32, outer surfaces 38 slide across inner surfaces 36 so as to shear occlusive material within the vasculature therebetween. In some cases, direct engagement between the inner basket and the surrounding tissues between the struts of the outer basket may also provide some shearing

and/or abrasion of occlusive mater.

[0035] The drive shaft may be axially coupled to both the inner and outer baskets at distal portions 26. This allows concurrent and coordinated radial expansion of the inner and outer baskets so as to maintain sufficient proximity between the inner surface 36 and the outer surface 38 to provide the desired shearing effect. In the exemplary embodiment, drive shaft 32 comprises a tube having a guide wire lumen 40 and an outer helical pumping element 42. As described in detail in U.S. Patent 6702830, rotation of such a helical pumping element within an aspiration lumen 44 of catheter body 12 can draw and/or pump severed fragments of occlusive material, debris, and fluid proximally into and/or through the catheter body. This actively pumped aspiration may draw fluid proximally from within proximal portions 24 of baskets 18, 20, and/or radially inwardly and then proximally through one or more aspiration windows 46 about catheter body 12.

[0036] In some embodiments, at least one of the inner and outer baskets 18, 20 may have struts 30 which extend, at least in part, substantially axially. Preferably, at least one of the baskets will have struts 30, which wind primarily toward a first circumferential orientation 50 as the struts proceed distally, as can be understood with reference to Fig. 4. Such a consistent winding direction can be used to consistently urge sheared materials proximally, as can be understood with reference to the arrows illustrated in Fig. 3A. As inner and outer surfaces 36, 38 slide against each other, material which is severed between these cooperating surfaces can be urged proximally when the inner basket is rotated relative to the outer basket in the proper direction.

[0037] Figs. 3B and 3C illustrate a catheter having a shearing means similar to that of Fig. 3A, and also having an expansible distal covering 31 (Fig. 3B) or an expansible proximal covering 33 (Fig. 3C). Coverings 31, 33 comprise a porous or non-porous coverings or coatings carried on (and expansible with) the outer shearing member along some (but typically not all) of the expansible portion of baskets 18, 20. Coatings 31, 33 may inhibit embolization of fragmented occlusive material, constrain a treatment fluid or fluid stream, inhibit injury to the venous valves and the like. Coverings 31, 33 extend between adjacent struts of a shearing member or positioning cage and accommodate radial expansion of the shearing member or positioning cage, the covering optionally being made from a PTFE woven material, filter material (metallic or polymeric), braid material (metallic or polymeric), mesh, polymeric coatings, and the like. The coatings may be applied to the outer basket through a dipping, filament winding or braiding process, or the like. Alternatively, the coverings may be applied to the outer basket using cyanoacrylate or other adhesives, thread or suturing, welding or bonding, or the like.

[0038] Referring now to Figs. 5 and 6, the basket structure embodying the invention is illustrated in a perspective view and as a flat pattern, respectively. The flat pat-

tern of Fig. 6 graphically illustrates the configuration of the struts 30 as if basket 50 were cut along one side and unrolled. Such flat patterns are useful for fabrication and understanding the strut configuration.

[0039] As is clearly seen in Figs. 5 and 6, a local helical wind angle defined between struts 30 and an axis 52 of basket 50 can vary along the axis. Preferably, a helical angle 54 along a central portion of struts 30 is significantly greater than a helical angle 56 near proximal and distal portions 24, 26. In other words, a pitch of struts 30 may vary locally along the axis of basket 50, with the pitch generally being greater adjacent the proximal and distal portions 24, 26. In the exemplary embodiment illustrated in Figs. 5 and 6, the pitch varies according to a sinusoidal function in which the period in the central 1/3 of the axial strut length is 1/2 the period on the proximal and distal thirds. Advantageously, such enhanced central helical winding angles help to avoid circumferential distortion of struts 30 when axis 52 is deflected laterally, so that uneven separation between the struts during axial bending is inhibited.

[0040] Referring now to Fig. 7, at least one of inner and outer baskets 18, 20 may include struts 30 having one or more circumferential protrusions 62. Struts 30 of basket 60 can define pockets which effectively capture occlusive material against the struts of the cooperating basket. This can help avoid excessively axial sliding of material for which shearing is desired, as the material will be caught at a pocket or protrusion between the cooperating shearing struts. This can be understood by imagining a pencil which is to be sheared between the cooperating surfaces of a pair of scissors. The pencil may slide along straight cooperating shearing surfaces. Such sliding may be inhibited by forming a protrusion and/or pocket to capture the pencil along an edge of one or both shearing members.

[0041] A still further alternative basket 70 is illustrated in Fig. 8. In this embodiment, one or more circumferential members 72 extend between adjacent struts 30 adjacent proximal and/or distal portions 24, 26. Circumferential member 72 can allow some expansion at the ends, and can help inhibit entraining structures which are disposed axially of the shearing baskets. For example, circumferential member 72 may help avoid severing valves within blood vessels. A variety of alternative circumferential members might be used, including expandable and/or elastomeric webs, braided meshes, or the like.

[0042] The shearing baskets may be formed of a metal, optionally comprising a superelastic metal, such as Nitinol®, Elgiloy®, or the like. Alternative basket materials may include stainless steel or other high strength metals, and the baskets may comprise a polymer in some embodiments. Optionally, struts 30 may comprise wire with wire struts often being affixed at the proximal and distal portions 24, 26. In the exemplary embodiment, the shearing baskets are formed from a continuous material extending along proximal portion 24, along struts 30, and along distal portion 26. The struts may have a circumfer-

ential width in a range from about 0.1mm (0.004") to about 2.5mm (0.100"), preferably having a width from about 0.15mm (0.006") to about 0.64mm (0.025"). The radial thickness of the struts will typically be in a range from about 0.03mm (0.001") to 1.3mm (0.05"), preferably being in a range from about 0.08mm (0.003") to about 0.64mm (0.025"). The baskets may be formed by selectively cutting a tube so as to define the struts, often by use of photoetch processing, laser cutting, waterjet abrasion, or EDM techniques.

[0043] Referring now to Figs. 9-11, coupling of drive shaft 32 and catheter body 12 to inner and outer shearing baskets 18, 20 can be understood. Adjacent proximal end 24, catheter 12 is axially and rotationally affixed to outer basket 20, as illustrated in Figs. 9 and 10. Drive shaft 32 rotates within aspiration lumen 44 of catheter body 12, and the drive shaft may have a helical pumping member 42. Pumping member 42 acts as an Archimedes screw, urging fluid and debris within proximal portion 24 of inner basket 18 proximally, and/or entraining fluid radially through aspiration windows 46.

[0044] Inner cutter 18 is rotationally affixed to drive shaft 32 adjacent portion 26, as illustrated in Fig. 11. Inner basket 18 is rotatable within proximal portion 24 of outer basket 20, and axial movement of the inner basket within the outer basket is limited by proximal cooperating thrust bearing surfaces 80, as seen in Figs. 9 and 10. Similarly, distal portion 26 of outer basket 20 is axially coupled to drive shaft 32 and inner basket 18 by distal thrust bearing surfaces 82, as illustrated in Fig. 11. A nose cone 84 presents an atraumatic distal tip adjacent the distal port of guidewire lumen 40.

[0045] As can now be understood with reference to Figs. 9-11, rotation of drive shaft 40 results in rotation of inner basket 18 within outer basket 20. Translating drive shaft 40 proximally within catheter 12 can result in radial expansion of the shearing baskets, as the cooperating distal thrust bearing surfaces 82 decrease the overall length of the shearing baskets. Separate thrust bearing surfaces might be coupled to independently axially movable structures so as to effect independent radial expansion of the baskets.

[0046] The structure and use of proximal housing 22 can be more clearly understood with reference to Figs. 12 and 13. Housing 22 contains a motor drivingly engaging drive shaft 32 within catheter body 12. The motor may be actuated by a drive actuator 88, with the drive actuator optionally effecting shearing motion of the inner basket and urging the sheared debris proximally when the actuator is moved in a first direction. When drive actuator is moved in a second direction, drive shaft 32 may rotate in an alternative direction, which may help free a jammed inner cutting member, or the like. An aspiration port 90 may be coupled to a vacuum source, such as a lockable syringe, a vacuum pump, or the like. A vacuum actuator 92 may provide momentary aspiration. Linear actuation of the drive shaft 32 may be provided by a linear actuator 34 (See Fig. 1) coupled to the drive shaft using thrust

bearings and axially slidable engagement of drive splines, or the like.

[0047] Referring now to Figs. 14-17, catheter 10 will generally be introduced into a blood vessel B over a guidewire GW using a conventional percutaneous or cut-down technique. Optionally, a portion of the blood vessel encompassing the target occlusive material may be isolated from surrounding blood flow. Such isolation may be provided by using a balloon guidewire and/or a sheath disposed around catheter body 12, with the sheath having an expandable member such as an annular balloon. Hence, isolation may be provided proximally and/or distally of an occlusive material O within a blood vessel wall W. Inner and outer baskets 18, 20 may be inserted and positioned adjacent the targeted occlusive material O while the baskets are in a low profile configuration, optionally using a remote imaging modality such as fluoroscopy, ultrasound, or the like.

[0048] As illustrated in Fig. 15, once catheter 10 has been appropriately positioned, drive shaft 32 may be translated proximally relative to catheter body 12 so as to radially expand inner and outer baskets 18, 20. Where the inner and outer baskets are biased to expand resiliently, drive shaft 32 may be released to allow the baskets to expand. Where the baskets are biased to a configuration smaller than the desired deployed configuration, the drive shaft may be urged proximally relative to catheter body 12 so as to overcome the resilience of the basket structures. Advantageously, the overall size of the cooperating shearing members may be selected by selectively axially positioning the drive shaft relative to the surrounding catheter body. This helps provide accurate control over the depth of material sheared from wall W.

[0049] Once the positioned catheter is properly expanded to the desired size, rotation of the inner basket 18 is initiated by actuation of drive actuator 88 of the proximal housing 22. This results in both shearing of occlusive material O from wall W, and in urging of the severed debris in a proximal direction (effected both by the crossing angle of the struts 30 and pumping of the helical member of drive shaft 32. An aspiration pressure differential may also be applied via proximal housing 22 as described above so as to avoid release of debris within the blood vessel.

[0050] As illustrated in Fig. 16, catheter 10 may advanced distally over guidewire GW within the vessel wall W during rotation of inner basket 18. Outer basket 20 slides distally against the vessel wall substantially without rotating, thereby providing an incremental and controlled shearing action which can follow axial bends of the natural or artificial blood vessel B. The amount of occlusive material O removed from vessel wall W at a particular location may depend on the expanded size of the cooperating shearing baskets at that location, on the speed of rotation of the inner basket, on the speed of axial translation of the shearing means, and on the total time and number of rotations of the inner basket at that location.

[0051] For relative soft occlusive material O, such as

clot material, the proximal shearing action of the struts may, at least in part, draw the occlusive material proximally from along the vessel wall into the interior of the baskets, as can be understood with reference to Fig. 17. Similarly, rotation of the helical struts 30 of inner basket 18 may help draw catheter 10 distally within blood vessel B.

[0052] As can be understood with reference to Fig. 17, serrated circumferential surfaces 94 may improve shearing efficiency by limiting sliding of occlusive material O. Regardless, as the strut of inner basket 18 rotates relative to the struts of outer basket 20, occlusive material O protruding into an interior of the baskets from wall W is both severed and/or urged proximally.

[0053] A variety of adaptations and modifications on the structures and methods described herein may be provided. For example, a kit may include some or all of the components of catheter 10 together with instructions for their use according to one or more of the methods described herein. Proximal end or distal portions 24, 26 of the inner and/or outer baskets may comprise a serpentine circumferential member, thereby allowing that portion to be expanded radially during assembly of catheter 10. It may be advantageous to at least slightly bias struts 30 radially outwardly so as to facilitate initial axial compression of the baskets. While the present invention has been described with reference to removal of clot, plaque, hyperplasia, or other occlusive material of a blood vessel, the structures and methods of the present invention may find applications for removing occlusive material from a wide variety of alternative body structures and lumens, including the fallopian tubes, genitourinary tract (for example, for treatment of benign prostatic hyperplasia, and the like), gastrointestinal tract, and the like.

[0054] A positioning cage catheter 120 which is particularly beneficial for treatment of blood vessels having a total occlusion (when it is difficult or impossible to access the entire treatment site with a standard guidewire) is illustrated in Figs. 18A and 18B. Many of known intraluminal therapies require that (or are facilitated when) the lumen has a significant open cross section, without an excessively tortuous luminal path, to allow the guide structure to be placed across the occlusion.

[0055] It should be noted that the term total occlusion may refer to any substance or anatomic morphology that acts to severely occlude a body conduit such that it is difficult to pass a wire from proximal end of the occlusion to the distal end. Depending on the type of material occluding the body conduit (soft plaque, calcified plaque, thrombus, fibrin, clot, intimal hyperplasia, in-stent restenosis, fatty tissue etc.) some occlusions may be more severe than others but all are included in the scope of the present invention when there may be some difficulty passing a guidewire therethrough.

[0056] Cage 110 may be formed of multiple straight wires or struts 111, or multiple curved wires or struts 112 formed into a helix as depicted in Fig. 18B. It is noted that a double wire (not shown) may also be employed to

form the cage structure. These cage structures are fixedly attached to a catheter body 113, having a distal tip 114 accommodating passage of a guidewire through lumen 115.

[0057] In an exemplary embodiment, catheter system 120 comprises a positioning cage such as described one of those described above, or such as those in related PCT Patent Application No. WO 2001/15759. A guidewire such as the described in U.S. Patent 6663613 (vibrating guidewire) or U.S. Patent 6287271, or in some cases such as those readily available from various manufacturers (TERUMO, CORP./BOSTON SCIENTIFIC, Natick, MA, GUIDANT, CORP., Indianapolis, IN, or PERCUSURGE, Sunnyvale, CA) may be used within catheter system 120, as will be understood from the following description. Optionally, the positioning cage and the treatment catheter may be employed as an integral unit to both place the guidewire, and to perform the subsequent treatment. In such embodiments a device such as those described in U.S. Patent 6663613 and in WO 2001/15759, may be employed.

[0058] In use, the total occlusion access devices of the present invention may be inserted into a body conduit and advanced to the proximal side of the occlusion, either over a guidewire, or by just advancing the positioning cage to the treatment site, depending on the body lumen to be treated. Once at the treatment site, the positioning cage can be pushed against the occlusion. As will be described below, a guidewire or dottering device may be advanced from the cage through a lumen coaxial with the cage (and hence, substantially coaxial with the body lumen when the cage is expanded therein) to penetrate and/or pierce the occlusion. The combination action of the positioning cage asserting forces against the vessel wall and the occlusive material (optionally by rotating the cage or expanding the against the vessel wall), and the guidewire or dottering device probing against the occlusion; may work to tunnel the devices through the occlusion to the distalmost portion and beyond. The positioning cage may help to center the action of the dottering member and inhibit perforations through the vessel wall or other vessel wall damage.

[0059] The positioning cage may be part of a treatment catheter and therefore, once the guidewire is in place, the treatment catheter may be advanced to initiate removal of the occlusion. Depending on the occlusion to be treated, a distal protection device, such as a balloon fixed to a guidewire, a filter affixed to a guidewire, or the like, may be employed distal of the occlusion and expanded to minimize any embolization of clot or other material. In addition, an occlusion balloon or filter may be deployed proximal of the occlusion to isolate the lesion and allow the treatment device (or a separate structure) to infuse saline, contrast, pharmacologic agents such as tPA, ReoPro, IIB3A inhibitors and the like, or chemical ablation agents or acid solutions such as those described in PCT Application No. PCT/US99/15918 (WO 00/03651). The occlusive debris can be removed by ac-

tivating the shearing, macerating, and aspirating function of the device of the present invention as described above, and in PCT Application WO 2001/15759 and U.S. patent 6702830.

[0060] Referring now to Figs. 18C-F, the structure of an exemplary positioning cage catheter system 120a adjacent distal tip 114 is illustrated in more detail. Catheter system 120a includes inner and outer shearing members in the form of baskets 18,20, as described above, and can also include some or all of the catheter structures described above for selectively expanding the inner and/or outer baskets, for irrigating and/or aspirating fluids, for urging fluids and severed fragments proximally within the outer sheath, for isolating the body lumen proximally and/or distally of the shearing members, and the like.

[0061] To facilitate advancement of catheter system 120a distally for treatment of a total occlusion, a total occlusion penetrator is provided adjacent tip 114. In the embodiment of Figs. 18C-F, the penetrator is in the form of a distally exposed morcellator 122. Morcellator 122 comprises a circumferential series of helical cutters which may be rotationally coupled to inner shearing member 18 or may rotate independently of the shearing member. The cutters of morcellator 122 may extend distally of the distal portion of the outer shearing member 20 and/or distally of the inner tubular body which defines the guidewire lumen 115 sufficiently to allow the rotating cutters to advance into the occlusive material of a total occlusion when the morcellator rotates. Expansion of the shearing member can maintain separation between the advancing morcellator and the vascular walls, so that the expanded shearing member acts as a positioning cage. As described above, use of a morcellator in the form of one or more helical structures within a lumen (the lumen here defined by the distal portion of outer shearing member 20) can act as a pump or Archimedes screw to urge the occlusive material proximally.

[0062] In use (as illustrated in Fig. 19), the positioning catheter 120 is inserted into a vessel BV and advanced to the treatment site just proximal of total occlusion TO. Cage 110 may actually engage the occlusion TO and begin loosening the plaque or other material making up the occlusion. Furthermore cage may be manually rotated to further engage the occlusion. Once at the treatment site, guidewire GW may be optionally advanced out of the distal tip of the positioning catheter to contact and help fragment the occlusion TO, the guidewire optionally being adapted for use as an occlusion penetrator, as will be described below. As described above regarding Figs. 18C-E, a morcellator 122 may also be used as an occlusive material penetrator by rotating the distally exposed morcellator and advancing the catheter system to engage the rotating morcellator against the total occlusion TO. Catheter 120, guidewire GW, and/or morcellator 122 may be used in combination or in an alternating motions or cycles to create a pilot hole through the occlusion TO such that the guidewire GW may be placed through the

occlusion and advanced distally therebeyond.

[0063] An alternative positioning cage catheter system is schematically depicted in Fig. 20. Treatment catheter 130 comprises a proximal end having a handle 131 with an actuator knob 132 and a Y connection 133 to allow infusion and/or aspiration. A catheter shaft 113 extends distally from handle 131 toward a distal working end 134. Fig. 21 depicts the distal working end of treatment catheter 130, showing a positioning cage 110 attached at its proximal end to catheter shaft 113, and on its distal end to distal tip 114. Distal working end 134 further comprises a drive shaft 141 with an optional coiled mechanical pump 141' and a macerator 142 coiled therearound. A more detailed description of treatment catheter 130 may be found in related case WO 2001/95759.

[0064] In use, as illustrated in Fig. 22, treatment catheter 130 is inserted into the lumen of a vessel BV and advanced to the proximal portion of the treatment site. At this point the lesion can either be crossed mechanically (as described above regarding Fig. 19) and/or saline or other therapeutic agents may be infused (optionally via guidewire lumen 115, as shown in Figs. 18) to assist in dissolving, softening, and/or fragmenting the occlusive material. In some embodiments, such agent flow from the catheter system alone may be sufficient to allow a standard guidewire to be advanced through the occlusion. The remaining components of the catheter system may then be advanced over the guidewire and remove some or all of the occlusive material, as described above.

[0065] A standard or modified guidewire may be used to help form a pilot hole or passage for placement of a guide structure. In the exemplary embodiment, a dottering tool or dottering guidewire 151 can be centered within the lumen of the blood vessel BV by expanding cage 110. The centered dottering tool 151 may then be used as an occlusive material penetrator by advancing the dottering tool in a linear translating and/or cycling motion to begin formation of a pilot hole or pathway through the total occlusion. Although dottering guidewire 151 may have a structure similar to a standard guidewire, the dottering tool will optionally have a more rigid construction than a standard guidewire adjacent the distal end, and the distal portion of the dottering tool may also be able to assume a straight configuration with sufficient axial column strength for advancement of an atraumatic tip distally from the guidewire lumen of the catheter system and into the occlusive material. Once dottering tool 151 has formed a passage 153 through the total occlusion, other devices (such as standard guidewires, a balloon guidewire or other distal protection devices to inhibit embolisms and/or release of therapeutic agents distally of the total occlusion, and the like) may be advanced through the passage, or the dottering wire may be used as a guide structure.

[0066] Referring now to Figs. 22 and 23, centering cage or basket 110 can provide centering of guidewire lumen 115. Centering of this coaxial lumen can help protect the vessel wall from mechanical injury imposed by

dottering device 151. Dottering device 151 may be cycled axially mechanically or using an axial drive motor, and may also be rotated manually or by drive motor. The centered guidewire lumen, which should be substantially coaxial with the vessel, may also be used for infusion of any of a variety of fluids. It may be advantageous to locally deliver (via guidewire lumen 115 or via some other infusion pathway) a thrombolytic agent having an enzymatic action with breads down fibrin clot matrix (such as Alteplase, tPA, Activase, Tenecteplase, TNK, and TNKase from Genentech, Inc.; Anistreplase a-SK, and Eminase from Roberts Pharmaceuticals; Reteplase, r-PA, and Retavase from Centocor, Inc.; Streptokinase, SK, and Streptase from AstraZeneca, Inc.; and/or Abbokinase, from Abbott, Inc. In some embodiments, a GP IIb/IIIa inhibitor, which inhibits the fibrogen binding site of platelet membrane, may be locally delivered. Suitable GP IIb/IIIa inhibitors may include Abciximab and ReoPro from Centocor, Inc.; Tirofiban and Aggrastat from Merck, Inc.; Eptifibatide and Integrelin from Cor Therapeutics, Inc.; Bitistatin, Kistrin, and Aspirin. Still further active agents might be used, including anti-thrombin agents and agents directed toward prevention of restenosis (to inhibit coagulation and/or decreasing smooth muscle proliferation and migration), such as Heparin, LMW, enoxaparine or Lovenox, dalteparin or Fragmin, ardeparin or Normoflo, Hirudin, Argatroban, PPACK, radioactive agents, nitrate, HA 1077, calcium antagonists, angiotensin converting enzyme inhibitor, anti-inflammatory agents, steroidal agents, anti-mitotic agents, HMG CoA reductase inhibitors, colchicine, angiopeptin, cytoclasin B, and the like. Gene therapy agents might also be locally delivered to inhibit restenosis and/or promote angiogenesis, with suitable agents optionally being delivered via plasmid vectors or by viral vectors, and suitable agents including genes relating to VEGF, C-myb, FGF, transforming growth factor b. endothelial growth factor, protooncogenes such as C-myc, C-myg, CDC-2, PCNA, and the like. Local delivery of chemotherapeutic agents (which are used to treat malignancies) may be employed, such as adriamycin or Doxorubicin. Imaging Media such as contrast media, radioactively labeled agents, or the like may be locally delivered, as might other agents such as plasminogen addative as an adjunct to thrombolytic therapy, immunosuppressive agents, Corazo'n material, lytics, saline, or the like.

[0067] As seen in Fig. 23, positioning cage 110 and dottering device 151 may be advanced simultaneously or in alternating partial steps into and through the total occlusion. Alternatively, dottering device 151 may be advanced through the total occlusion while the expanded positioning cage remains at a fixed location. Regardless, some penetrator structure of the catheter system will preferably advance until a passage 153 is formed through the total occlusion. Once an opening, propagation plane, or pathway has been formed through the occlusion TO, a guide structure may be passed distally along passage 153 beyond the total occlusion.

[0068] In addition to use of cage 110 to protect the vessel wall W from harm by positioning of the penetrator, the cage may be advanced against the proximal portion of the occlusion TO as shown in Fig. 24A (in which cage 110 is shown in a partially expanded configuration 110a) and then expanded (to a more fully expanded configuration 110b) to assist in propagating a passage, plane, or pathway through the occlusion, as shown in Fig. 24B. In other words, expansion of cage 110 may open up or propagate a cleavage plane to facilitate passing a guidewire or dottering device 51 using a wedge effect. This wedge effect may, of course, be combined with axial cycling of dottering device 51, rotation and advancement of a cutter, occlusive material agent dissolution, and any of the other mechanisms described herein. Similarly, the various occlusion treatment methods and structures described herein will generally be compatible for use in combination.

[0069] Figs. 25A-25B illustrate further steps in treatment of the occlusion (TO) once a guidewire has been passed distally. As illustrated, a distal protection member 155 is inserted over the guidewire (or is attached to the guidewire itself) through passage 153 and expanded distally of the occlusion. Distal protection member 155 inhibits distal flow beyond the occlusion and can help decrease or prevent embolization of material downstream of the treatment site. Distal member 155 may comprise an annular balloon fixed on a catheter or guidewire, a radially expandable filter, or any of a wide variety of flow and/or embolization inhibiting intraluminal structures. Optionally, an intravascular ultrasound (IVUS) sensor 157 may be carried by at least one of the components of the catheter system, optionally in a component which will traverse the occlusion such as the guidewire or dottering device 151 (or other penetrator), a shaft axially coupled to distal protection member 155, or the like. Alternatively, IVUS capabilities may be incorporated in one or more of the other catheter system components, or may be provided by a dedicated structure that can be advanced through a lumen of the catheter system or independent thereof. Such IVUS capabilities may be useful for planning an occlusion therapy, for monitoring progress of the therapy, and/or for verifying the effectiveness of the therapy.

[0070] Once flow distal of the occlusive material OM is inhibited, treatment of the lesion can continue using any of a wide variety of modalities of treatment such as atherectomy, endarterectomy, infusion of occlusive material removal flow or active agents, and the like. Alternatively, as shown in Fig. 25B, a proximal occluding member 159 may also be inflated or expanded to isolate the treatment site. Proximal occluding member may again comprise a balloon or embolic filter carried on the outer surface of shaft 113 or on an outer sheath 161, with occlusion and fluid isolation allowing the infusion of various treatment modalities such as saline, contrast, pharmacologic agents such as tPA, ReoPro, IIB3A inhibitors and the like, or chemical ablation agents or acid solutions

such as those listed above regarding Figs. 22 and 23, and/or those described in PCT Application No. PCT/US99/15918 (Publication No. WO 00/03651). In the case of any acidic compounds, it is beneficial to fully contain the compounds infused within the treatment site, and to expeditiously remove and aspirate the dissolved material.

[0071] In Figs. 25B and C, the treatment catheter 130, and specifically the mechanical pump (141 and 141') is used to remove some or all remaining occlusive material OM, including thrombus, plaque, fibrin, clot and the like, while still protecting the vessel wall. Fluid may optionally be circulated by, for example, infusion via lumen 115 while aspirating via a lumen 163 of shaft 113, the aspiration often being assisted by rotation of the Archimedes screw pump 141' within the aspiration lumen as described above. A vacuum source may be applied to the aspiration lumen via the proximal housing or only a proximal pump may be included, and some embodiments of the occlusion removal and access catheters described herein may not include an integral mechanical pump disposed in a distal lumen of the catheter system. The catheter is then removed and the vessel may then be further treated with a liner, stent, coated stent, stent-graft, or the like, as is taught by the prior art and is known to those skilled in the art.

[0072] The use of the occlusive material removing catheter system embodiment of Figs. 18C-E can be understood with reference to Fig. 26. Once again, a positioning cage 110 is located on the distal portion of a treatment catheter 120a. Treatment catheter 120a may include an axially moveable driveshaft 165, the cutters 122 may be axially affixed in a distally exposed configuration, or a distal cover may be removed *in situ* from cutters 122 of the morcellator. Regardless, the driveshaft 165 can be advanced into the occlusion TO while the driveshaft and (and the cutters carried thereon) rotate to create the desired pilot hole, propagation plane or passage for a guidewire or other guide device. Alternatively, the inner or outer cage may be translated distally and/or in tension to distally expose a morcellator that drills similarly into and/or through the total occlusion TO. Hence, a variety of related embodiments will be clear to those of skill in the art in light of the disclosure herein. For example, rather than a morcellator formed of helical cutters extending distally from within a lumen, the penetrator may comprise a blunt dissection tool distally extending from a fixed outer or rotating inner cage, a cutter in the form of a spinning burr or screw extending distally from a rotating inner cage, or the like.

[0073] It should be noted that any of the method steps or devices used in one method description may be interchanged with method steps of another description and still be in the scope of the present invention. For example, the isolation balloon or distal protection device may be used in conjunction with the positioning cage catheter 120, and well as through and in conjunction with treatment catheter 130. Furthermore, the terms pilot hole and

propagation plane are used to refer to any path that is created through a occlusion (TO), either through the center of the vessel lumen, or to one side or the other around the circumference of the vessel lumen.

[0074] While the exemplary embodiments have been described in some detail, by way of example and for clarity of understanding, a variety of adaptations, changes, and modifications will be obvious to those of skill in the art. Hence, the scope of the present invention is limited solely by the appended claims.

Claims

1. A vascular obstruction removal catheter comprising:
 - a flexible tubular body having a proximal end and a distal end;
 - an outer shearing member attached near the distal end, the outer member having a perforate inner surface;
 - an inner shearing member rotatably disposed within the outer member, the inner member having a proximal portion, a distal portion, and a circumferential series of struts extending therebetween along a longitudinal axis of the inner shearing member, the struts sliding along the inner surface of the outer shearing member when the inner shearing member rotates;
 - wherein the inner and outer shearing members are expansible between an unexpanded state and an expanded state, wherein the struts are helically oriented, and **characterized in that** in the unexpanded state a local pitch of the struts varies along the longitudinal axis of the inner shearing member.
2. The vascular obstruction removal catheter of claim 1, wherein the inner member is adapted to rotate about an axis, and wherein the inner and outer shearing bodies are sufficiently flexible to deflect the axis laterally when the outer shearing member engages a surrounding vessel and the inner member rotates therein.
3. The vascular obstruction removal catheter of any of the preceding claims, wherein the struts comprise helical struts and uniformly coil distally toward a first circumferential orientation so that rotation of the inner shearing member toward the first circumferential orientation consistently urges sheared occlusive material proximally.
4. The vascular obstruction removal catheter of any of the preceding claims, wherein the inner shearing member comprises tube material, the struts being separated by laser cut surfaces between adjacent tube material portions.
5. The vascular obstruction removal catheter of claim 4, further comprising an expansible covering extending between adjacent struts of the outer shearing member to capture debris.
6. The vascular obstruction removal catheter of claim 4, wherein the outer shearing member comprises outer tube material having a proximal outer portion, a distal outer portion and a circumferential series of outer struts extending helically therebetween, the struts being separated by laser cut outer surfaces between outer adjacent tube material portions.
7. The vascular obstruction removal catheter of any of the preceding claims, wherein the struts are affixed together at the proximal portion and at the distal portion, and wherein the struts flex independently therebetween.
8. The vascular obstruction removal catheter of any preceding claim, wherein the local pitch increases toward the proximal and distal portions sufficiently to inhibit excessive separation between adjacent struts when the outer shearing member flexes axially.
9. The vascular obstruction removal catheter of claim 8, wherein the struts have protrusions which inhibit sliding of obstructive material axially between cooperating edges of the inner and outer shearing bodies.
10. The vascular obstruction removal catheter of any of the preceding claims, wherein at least one expansion actuator extends proximally from the shearing members so that the inner and outer shearing members can be radially expanded *in situ*.
11. The vascular obstruction removal catheter of claim 10, wherein axial translation of an expansion actuator selectively radially expands the inner and outer shearing members concurrently.
12. The vascular obstruction removal catheter of any of the preceding claims, further comprising a distally oriented occlusion penetrator adjacent the distal end.
13. The vascular obstruction removal catheter of claim 12, wherein the occlusion penetrator comprises at least one end cutter that rotates with the inner shearing member and is exposed distally of the outer shearing member to advance the shearing members within a body lumen distally through occlusive material.
14. The vascular obstruction removal catheter of claim 12, wherein the occlusion penetrator comprises a shaft extendable distally of the shearing members,

the shaft axially cycleable through occlusive material without penetrating through a vessel wall.

15. The vascular obstruction removal catheter of any of the preceding claims, further comprising an intravascular ultrasound sensor to measure of vascular obstructions for removal. 5
16. A method for forming a vascular obstruction removal catheter, the method comprising: 10
- providing a first tube having a proximal end and a distal end with a central region therebetween, the tube comprising a tube material;
- cutting axially along the central region of the first tube so as to define a circumferential series of independent struts along a longitudinal axis of the first tube to define a first cage, the struts comprising the tube material; 15
- positioning the first cage coaxially with a second resiliently deformable cage; 20
- attaching a drive for rotating at least one of the cages within a blood vessel for shearing of obstructive material between the cages;
- wherein the cages are expansible between an unexpanded state and an expanded state, wherein cutting of the struts is such that the struts are helically oriented and in the unexpanded state a local pitch of the struts varies along the longitudinal axis of the first tube. 25
17. A shearing member for use in a catheter device for removal of obstructive material from the lumen of a body conduit, said component comprising: 30
- first and second end portions having a longitudinal axis therebetween;
- a middle portion having at least one second cross sectional diameter and further comprising one or more flexible struts around the circumference of said longitudinal axis and extending between, but not along, said first end portion and said second end portion; and 35
- wherein said middle portion and said end portions are formed from a continuous tube that is expansible between an unexpanded state and an expanded state, wherein the struts are arranged in a helical orientation and **characterized in that** in the unexpanded state a local pitch of the struts varies along said longitudinal axis. 40
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Patentansprüche

1. Katheter zum Entfernen einer vaskulären Obstruktion, der aufweist: 55
- einen biegsamen röhrenförmigen Körper mit ei-

nem proximalen Ende und einem distalen Ende; ein äußeres Scherteil, das nahe dem distalen Ende befestigt ist, wobei das äußere Teil eine perforierte Innenfläche hat;

ein inneres Scherteil, das drehbar in dem äußeren Teil angebracht ist, wobei das innere Teil einen proximalen Abschnitt, einen distalen Abschnitt und eine Reihe umlaufender Streben hat, die sich entlang der Längsachse des inneren Scherteils dazwischen erstrecken, wobei die Streben entlang der Innenfläche des äußeren Scherteils gleiten, wenn sich das innere Scherteil dreht;

wobei die inneren und äußeren Scherteile zwischen einem nicht aufgeweiteten Zustand und einem aufgeweiteten Zustand aufgeweitet werden können, wobei die Streben schraubenförmig ausgerichtet sind,

dadurch gekennzeichnet, dass

im nicht aufgeweiteten Zustand eine lokale Steigung der Streben entlang der Längsachse des inneren Scherteils variiert.

2. Katheter zum Entfernen einer vaskulären Obstruktion nach Anspruch 1, wobei das innere Teil so ausgelegt ist, dass es sich um eine Achse dreht, und wobei die inneren und äußeren Scherkörper ausreichend biegsam sind, um die Achse seitlich abzulenken, wenn das äußere Scherteil in ein umgebendes Gefäß eingreift und das innere Teil sich darin dreht.
3. Katheter zum Entfernen einer vaskulären Obstruktion nach einem der vorhergehenden Ansprüche, wobei die Streben schraubenförmige Streben aufweisen und sich gleichmäßig distal in eine erste Umfangsausrichtung winden, so dass eine Drehung des inneren Scherteils in die erste Umfangsausrichtung abgeschorenes Okklusionsmaterial beständig nach proximal drängt.
4. Katheter zum Entfernen einer vaskulären Obstruktion nach einem der vorhergehenden Ansprüche, wobei das innere Scherteil Schlauchmaterial aufweist, wobei die Streben durch Laserschnittflächen zwischen benachbarten Schlauchmaterialabschnitten getrennt sind.
5. Katheter zum Entfernen einer vaskulären Obstruktion nach Anspruch 4, der des Weiteren eine aufwekbare Abdeckung aufweist, die sich zwischen benachbarten Streben des äußeren Scherteils erstreckt, um Ablagerungen zu erfassen.
6. Katheter zum Entfernen einer vaskulären Obstruktion nach Anspruch 4, wobei das äußere Scherteil ein äußeres Schlauchmaterial mit einem proximalen äußeren Abschnitt, einem distalen äußeren Abschnitt

und einer Reihe umlaufender äußerer Streben aufweist, die sich schraubenförmig dazwischen erstrecken, wobei die Streben durch Laserschnitt-Außenflächen zwischen benachbarten äußeren Schlauchmaterialabschnitten getrennt sind.

7. Katheter zum Entfernen einer vaskulären Obstruktion nach einem der vorhergehenden Ansprüche, wobei die Streben an dem proximalen Abschnitt und an dem distalen Abschnitt zusammen befestigt sind, und wobei sich die Streben dazwischen unabhängig biegen. 5
8. Katheter zum Entfernen einer vaskulären Obstruktion nach einem der vorhergehenden Ansprüche, wobei sich die lokale Steigung zu den proximalen und distalen Abschnitten hin ausreichend vergrößert, um eine übermäßige Trennung zwischen benachbarten Streben zu verhindern, wenn sich das äußere Scherteil axial biegt. 10 15 20
9. Katheter zum Entfernen einer vaskulären Obstruktion nach Anspruch 8, wobei die Streben Vorsprünge aufweisen, die verhindern, dass störendes Material axial zwischen zusammenwirkenden Kanten der inneren und äußeren Scherkörper gleitet. 25
10. Katheter zum Entfernen einer vaskulären Obstruktion nach einem der vorhergehenden Ansprüche, wobei sich wenigstens ein Ausweitungs-Betätigungsmittel proximal von den Scherteilen erstreckt, so dass die inneren und äußeren Scherteile *in situ* radial aufgeweitet werden können. 30
11. Katheter zum Entfernen einer vaskulären Obstruktion nach Anspruch 10, wobei die axiale Translation eines Aufweitungs-Betätigungsmittels die inneren und äußeren Scherteile selektiv gleichzeitig aufweitet. 35
12. Katheter zum Entfernen einer vaskulären Obstruktion nach einem der vorhergehenden Ansprüche, der des Weiteren einen distal ausgerichteten Okklusions-Eindringkörper nahe dem distalen Ende aufweist. 40 45
13. Katheter zum Entfernen einer vaskulären Obstruktion nach Anspruch 12, wobei der Okklusions-Eindringkörper wenigstens einen Endschneider aufweist, der sich mit dem inneren Scherteil dreht und distal von dem äußeren Scherteil freiliegend ist, um die Scherteile in einem Körperlumen distal durch Okklusionsmaterial vorzuschieben. 50
14. Katheter zum Entfernen einer vaskulären Obstruktion nach Anspruch 12, wobei der Okklusions-Eindringkörper einen Schaft aufweist, der distal von den Scherteilen ausfahrbar ist, wobei der Schaft axial 55

durch Okklusionsmaterial zyklisch bewegt werden kann, ohne durch eine Gefäßwand zu dringen.

15. Katheter zum Entfernen einer vaskulären Obstruktion nach einem der vorhergehenden Ansprüche, der des Weiteren einen intravaskulären Ultraschallsensor aufweist, um vaskuläre Obstruktionen, die zu entfernen sind, zu messen.

16. Verfahren zum Ausbilden eines Katheters zum Entfernen einer vaskulären Obstruktion, wobei das Verfahren umfasst:

Bereitstellen eines ersten Schlauchs mit einem proximalen Ende und einem distalen Ende mit einem dazwischenliegenden Mittelbereich, wobei der Schlauch ein Schlauchmaterial enthält; axiales Schneiden entlang des Mittelbereichs des ersten Schlauchs, um eine Reihe unabhängiger Umfangsstreben entlang der Längsachse des ersten Schlauchs zu definieren, um einen ersten Käfig zu definieren, wobei die Streben das Schlauchmaterial aufweisen; Positionieren des ersten Käfigs koaxial mit einem zweiten elastisch verformbaren Käfig; Befestigen eines Antriebs zum Drehen wenigstens eines der Käfige in einem Blutgefäß zum Scheren von Obstruktionsmaterial zwischen den Käfigen; wobei die Käfige zwischen einem nicht aufgeweiteten Zustand und einem aufgeweiteten Zustand aufgeweitet werden können, wobei das Schneiden der Streben derart erfolgt, dass die Streben schraubenförmig ausgerichtet werden, und im nicht aufgeweiteten Zustand eine lokale Steigung der Streben entlang der Längsachse des ersten Schlauchs variiert.

17. Scherteil zur Verwendung bei einer Kathetervorrichtung zum Entfernen von Obstruktionsmaterial aus dem Lumen eines Körperkanals, wobei das Teil aufweist:

erste und zweite Endabschnitte mit einer dazwischenliegenden Längsachse; einen Mittelabschnitt mit wenigstens einem zweiten Querschnittsdurchmesser, der des Weiteren eine oder mehrere biegsame Streben um den Umfang der Längsachse herum aufweist, und der sich zwischen, jedoch nicht entlang, dem ersten Endabschnitt und dem zweiten Endabschnitt erstreckt; und wobei der Mittelabschnitt und die Endabschnitte aus einem durchgehenden Schlauch ausgebildet sind, der zwischen einem nicht aufgeweiteten Zustand und einem aufgeweiteten Zustand aufgeweitet werden kann, wobei die Streben in schraubenförmiger Ausrichtung angeordnet

sind,

dadurch gekennzeichnet, dass

im nicht aufgeweiteten Zustand eine lokale Steigung der Streben entlang der Längsachse variiert.

Revendications

1. Cathéter de retrait d'obstruction vasculaire comprenant :

un corps tubulaire souple ayant une extrémité proximale et une extrémité distale ;
un élément extérieur de cisaillement fixé près de l'extrémité distale, l'élément extérieur ayant une surface intérieure perforée ;
un élément intérieur de cisaillement disposé de manière rotative à l'intérieur de l'élément extérieur, l'élément intérieur ayant une partie proximale, une partie distale, et une série circonférentielle d'entretoises s'étendant entre celles-ci le long d'un axe longitudinal de l'élément intérieur de cisaillement, les entretoises glissant le long de la surface intérieure de l'élément extérieur de cisaillement lorsque l'élément intérieur de cisaillement tourne ;
dans lequel les éléments intérieur et extérieur de cisaillement sont expansibles entre un état non expansé et un état expansé, dans lequel les entretoises sont orientées de manière hélicoïdale, et **caractérisé en ce que** dans l'état non expansé, un pas local des entretoises varie le long de l'axe longitudinal de l'élément intérieur de cisaillement.

2. Cathéter de retrait d'obstruction vasculaire selon la revendication 1, dans lequel l'élément intérieur est adapté pour tourner autour d'un axe, et dans lequel les corps intérieur et extérieur de cisaillement sont suffisamment souples pour dévier l'axe latéralement lorsque l'élément extérieur de cisaillement vient en prise avec un vaisseau alentour et l'élément intérieur tourne dans celui-ci.

3. Cathéter de retrait d'obstruction vasculaire selon l'une quelconque des revendications précédentes, dans lequel les entretoises comprennent des entretoises hélicoïdales et sont embobinées uniformément de manière distale vers une première orientation circonférentielle de sorte que la rotation de l'élément intérieur de cisaillement vers la première orientation circonférentielle sollicite constamment la matière occlusive cisailée de manière proximale.

4. Cathéter de retrait d'obstruction vasculaire selon l'une quelconque des revendications précédentes, dans lequel l'élément intérieur de cisaillement com-

prend une matière en tube, les entretoises étant séparées par des surfaces coupées au laser entre des parties de matière en tube adjacentes.

5. Cathéter de retrait d'obstruction vasculaire selon la revendication 4, comprenant en outre une couverture expansible s'étendant entre des entretoises adjacentes de l'élément extérieur de cisaillement pour capturer les débris.
6. Cathéter de retrait d'obstruction vasculaire selon la revendication 4, dans lequel l'élément extérieur de cisaillement comprend une matière en tube extérieure ayant une partie extérieure proximale, une partie extérieure distale et une série circonférentielle d'entretoises extérieures s'étendant de manière hélicoïdale entre celles-ci, les entretoises étant séparées par des surfaces extérieures coupées au laser entre les parties de matière en tube extérieure adjacentes.
7. Cathéter de retrait d'obstruction vasculaire selon l'une quelconque des revendications précédentes, dans lequel les entretoises sont fixées ensemble au niveau de la partie proximale et au niveau de la partie distale, et dans lequel les entretoises fléchissent indépendamment entre celles-ci.
8. Cathéter de retrait d'obstruction vasculaire selon l'une quelconque des revendications précédentes, dans lequel le pas local augmente vers les extrémités proximale et distale suffisamment pour inhiber une séparation excessive entre les entretoises adjacentes lorsque l'élément extérieur de cisaillement fléchit axialement.
9. Cathéter de retrait d'obstruction vasculaire selon la revendication 8, dans lequel les entretoises ont des saillies qui inhibent le glissement axial de la matière obstructive entre les bords coopérants des corps intérieur et extérieur de cisaillement.
10. Cathéter de retrait d'obstruction vasculaire selon l'une quelconque des revendications précédentes, dans lequel au moins un actionneur d'expansion s'étend de manière proximale à partir des éléments de cisaillement de sorte que les éléments intérieur et extérieur de cisaillement peuvent être expansés radialement *in situ*.
11. Cathéter de retrait d'obstruction vasculaire selon la revendication 10, dans lequel la translation axiale d'un actionneur d'expansion provoque l'expansion, sélectivement et radialement, des éléments intérieur et extérieur de cisaillement de manière simultanée.
12. Cathéter de retrait d'obstruction vasculaire selon l'une quelconque des revendications précédentes, comprenant en outre un pénétrateur d'occlusion

orienté de manière distale adjacent à l'extrémité distale.

13. Cathéter de retrait d'obstruction vasculaire selon la revendication 12, dans lequel le pénétrateur d'occlusion comprend au moins un dispositif de coupe d'extrémité qui tourne avec l'élément intérieur de cisaillement et est exposé de manière distale par rapport à l'élément extérieur de cisaillement pour avancer les éléments de cisaillement à l'intérieur d'une lumière de corps de manière distale à travers la matière occlusive. 5
14. Cathéter de retrait d'obstruction vasculaire selon la revendication 12, dans lequel le pénétrateur d'occlusion comprend un arbre extensible de manière distale par rapport aux éléments de cisaillement, l'arbre étant axialement rotatif à travers la matière occlusive sans pénétrer une paroi de vaisseau. 10
15. Cathéter de retrait d'obstruction vasculaire selon l'une quelconque des revendications précédentes, comprenant en outre un capteur à ultrasons intravasculaire pour mesurer les obstructions vasculaires pour leur retrait. 20
16. Procédé pour la formation d'un cathéter de retrait d'obstruction vasculaire, le procédé comprenant : 25
 - la fourniture d'un premier tube ayant une extrémité proximale et une extrémité distale avec une région centrale entre celles-ci, le tube comprenant une matière en tube ; 30
 - la coupe, axialement, le long de la région centrale du premier tube, de manière à définir une série circonférentielle d'entretroises indépendantes le long d'un axe longitudinal du premier tube pour définir une première cage, les entretroises comprenant la matière en tube ; 35
 - le positionnement de la première cage coaxialement avec une deuxième cage élastiquement déformable ; 40
 - la fixation d'un système d'entraînement pour la rotation d'au moins l'une des cages à l'intérieur d'un vaisseau sanguin pour la coupe de matière obstructive entre les cages ; 45
 - dans lequel les cages sont expansibles entre un état non expansé et un état expansé, dans lequel la coupe des entretroises est telle que les entretroises sont orientées de manière hélicoïdale et dans l'état non expansé, un pas local des entretroises varie le long d'un axe longitudinal du premier tube. 50
17. Élément de cisaillement destiné à être utilisé dans un dispositif de cathéter pour le retrait de matière obstructive dans la lumière d'un conduit corporel, ledit composant comprenant : 55

des première et deuxième parties d'extrémité ayant un axe longitudinal entre celles-ci ;
 une partie centrale ayant au moins un deuxième diamètre transversal et comprenant en outre une ou plusieurs entretoises souples autour de la circonférence dudit axe longitudinal et s'étendant entre, mais pas le long de ladite première partie d'extrémité et de ladite deuxième partie d'extrémité ; et
 dans lequel ladite partie centrale et lesdites parties d'extrémité sont formées à partir d'un tube continu qui est expansible entre un état non expansé et un état expansé, dans lequel les entretroises sont agencées dans une orientation hélicoïdale et **caractérisé en ce que** dans l'état non expansé, un pas local des entretroises varie le long dudit axe longitudinal.

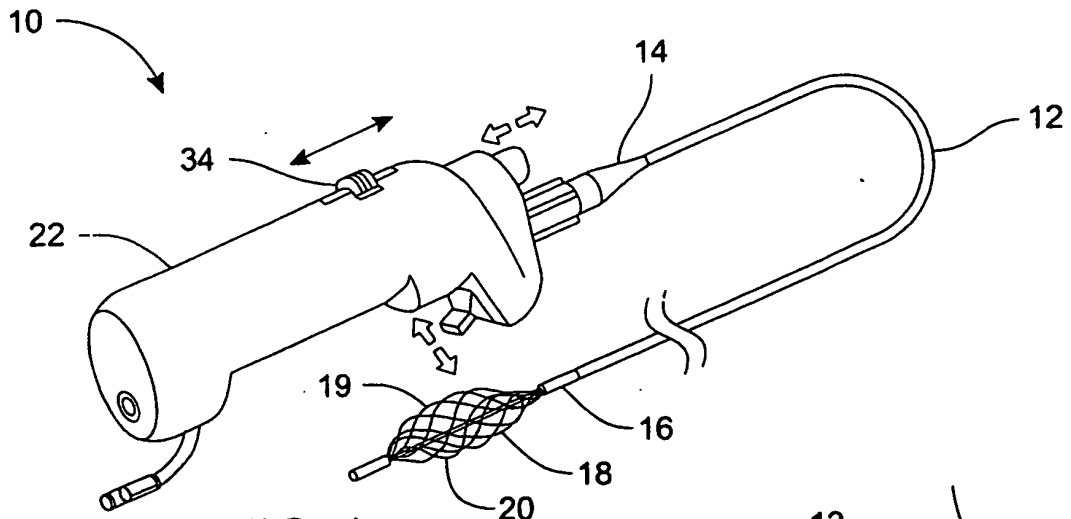


FIG. 1

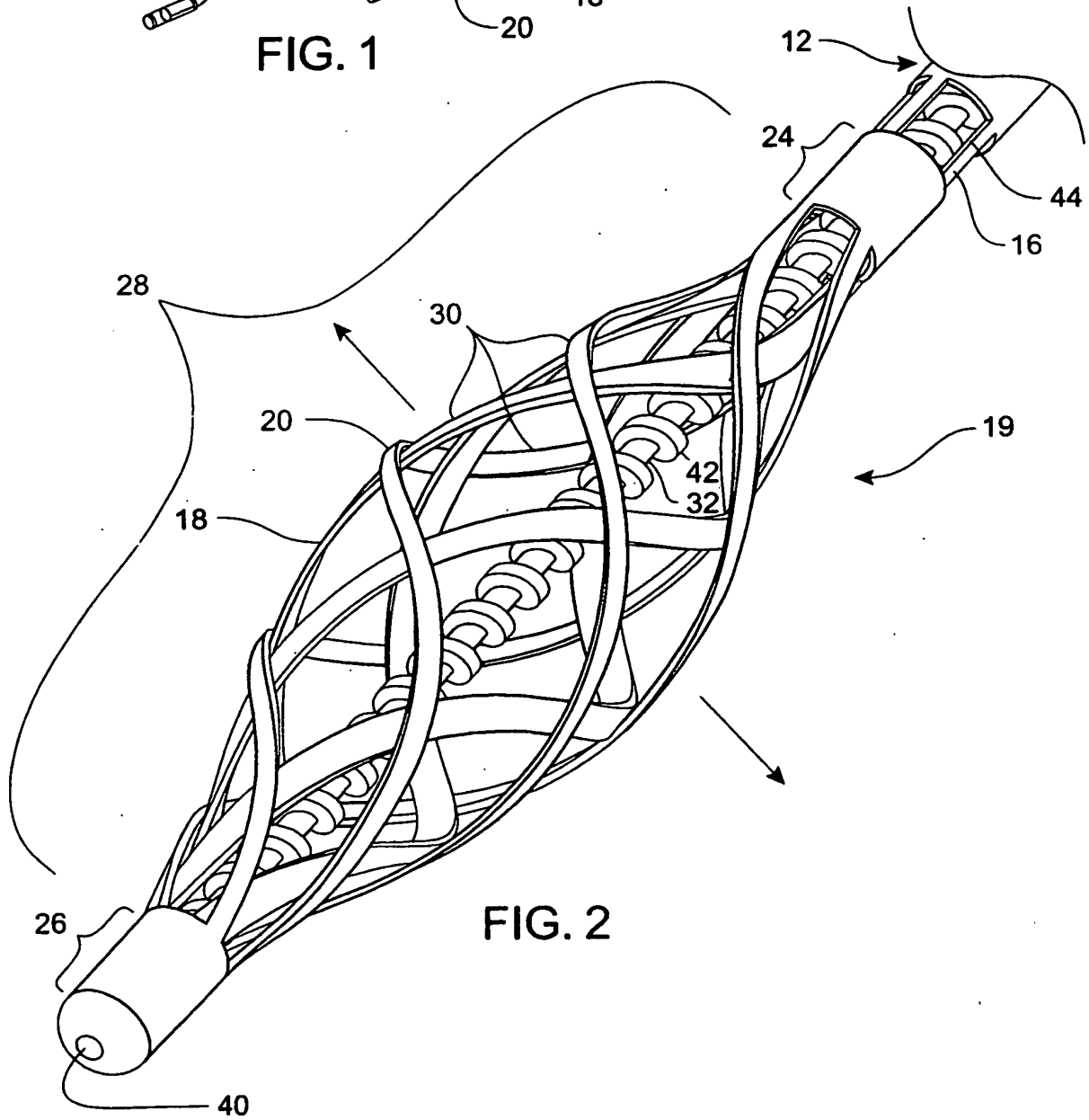
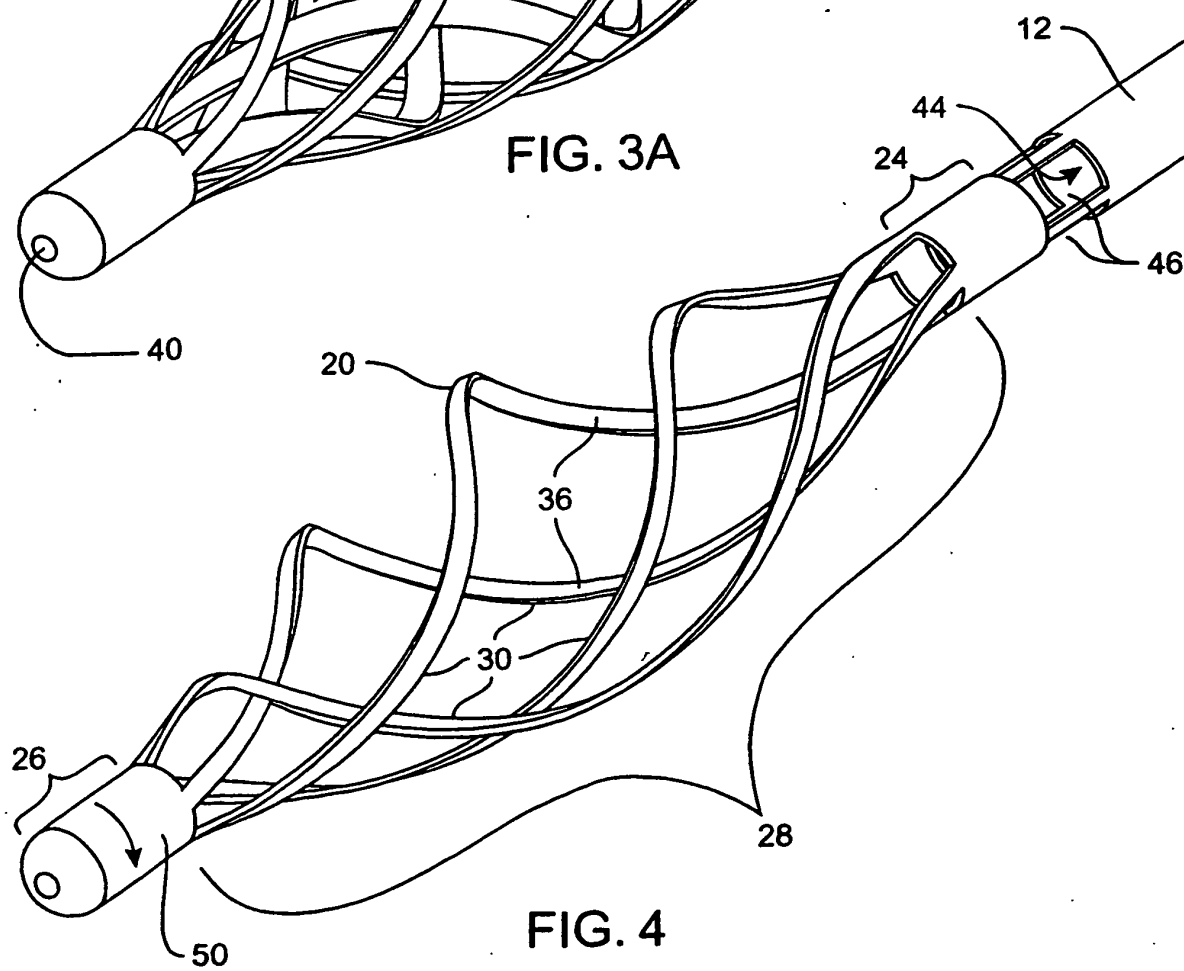
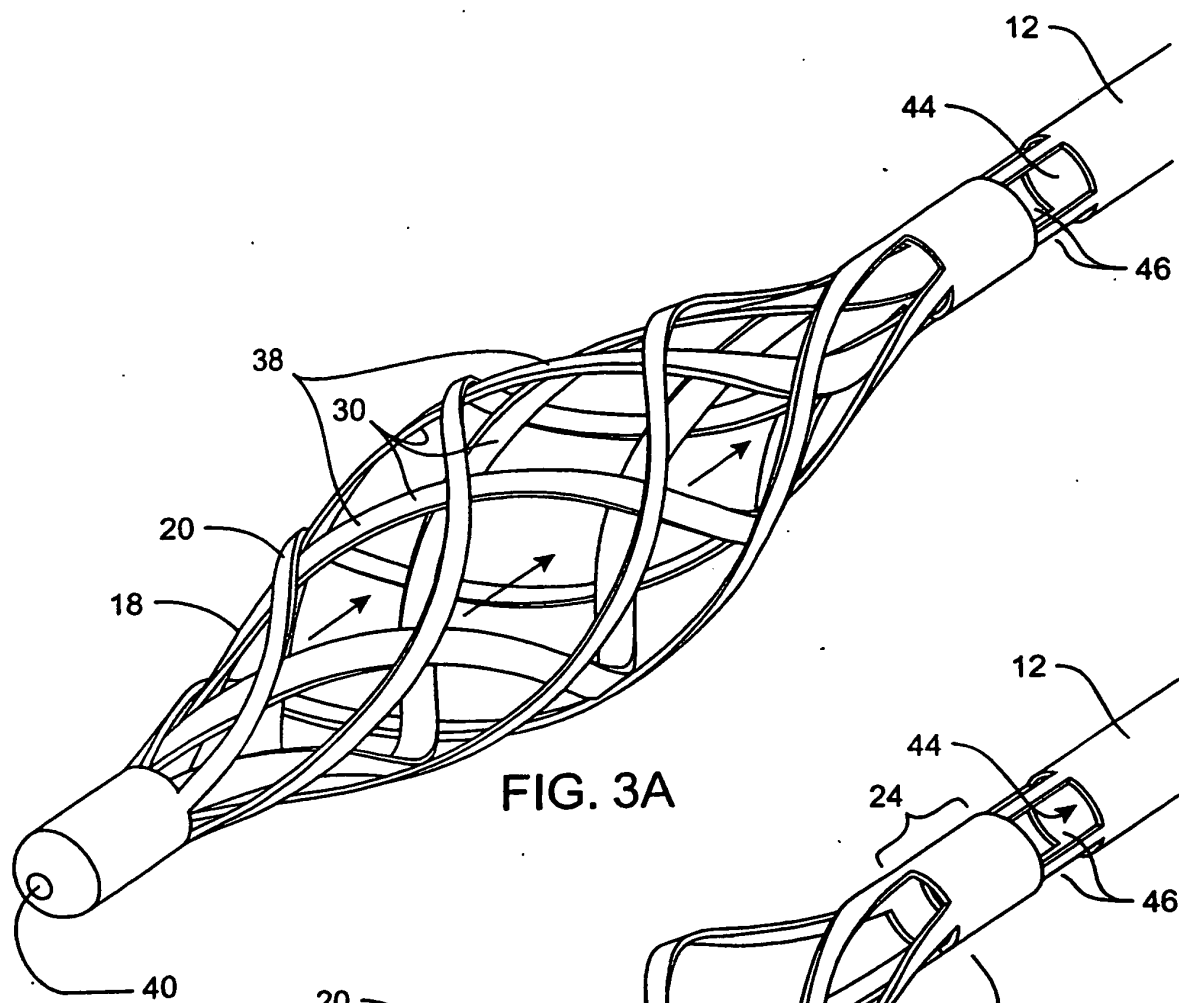


FIG. 2



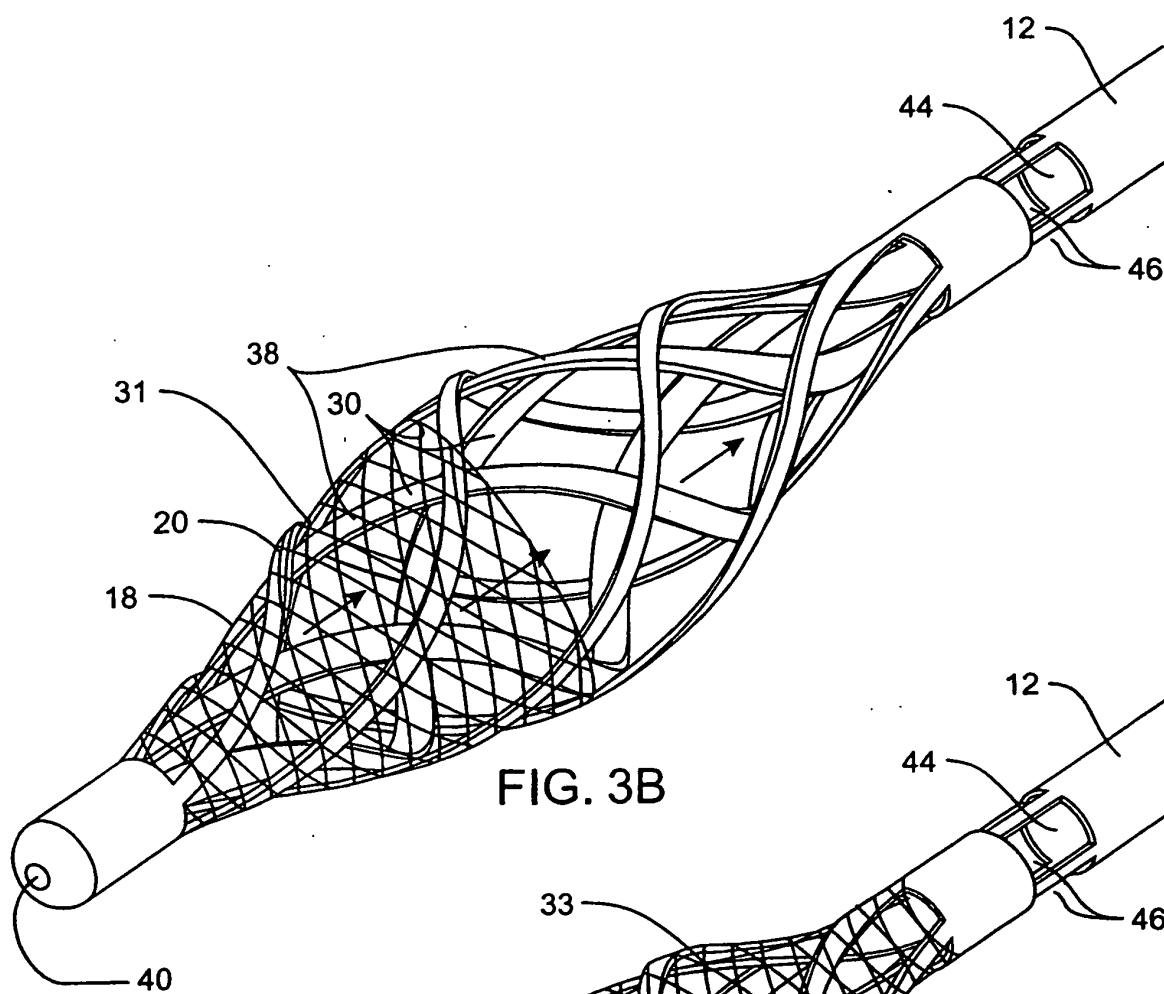


FIG. 3B

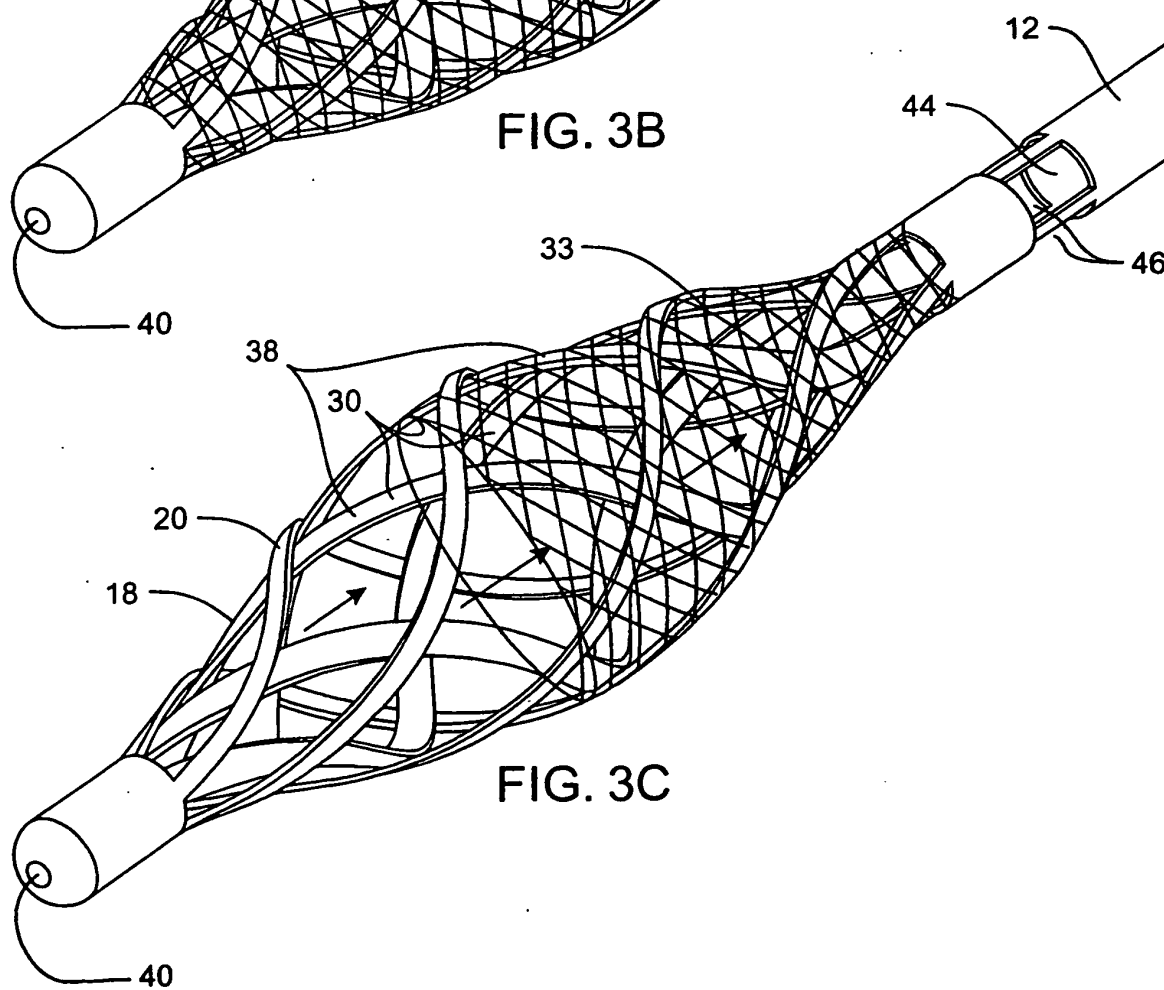
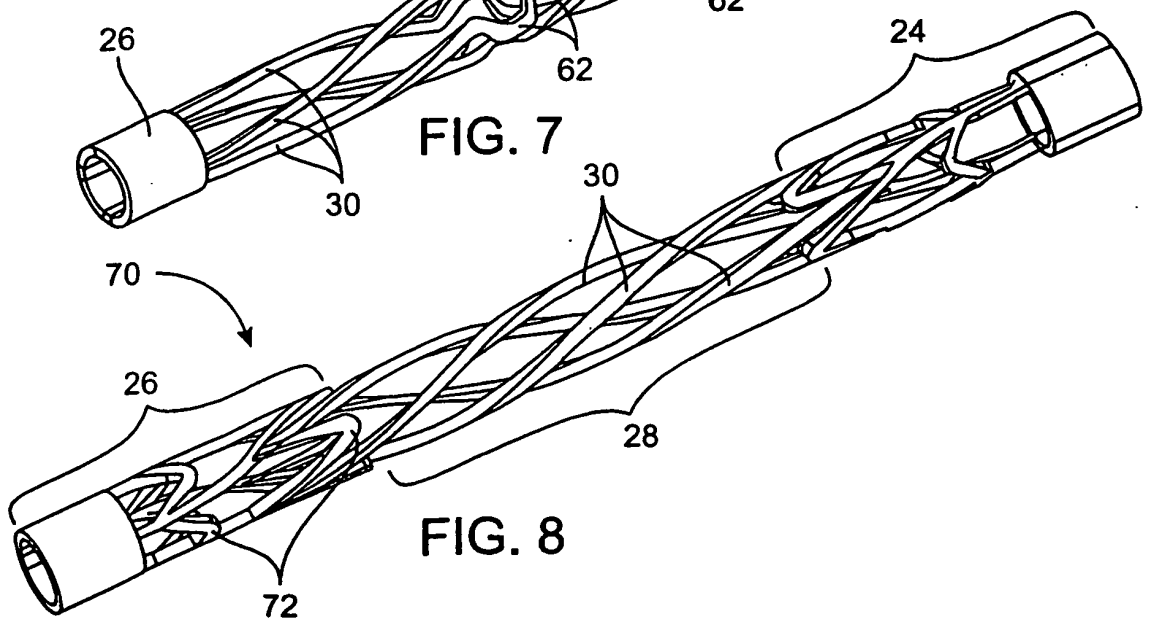
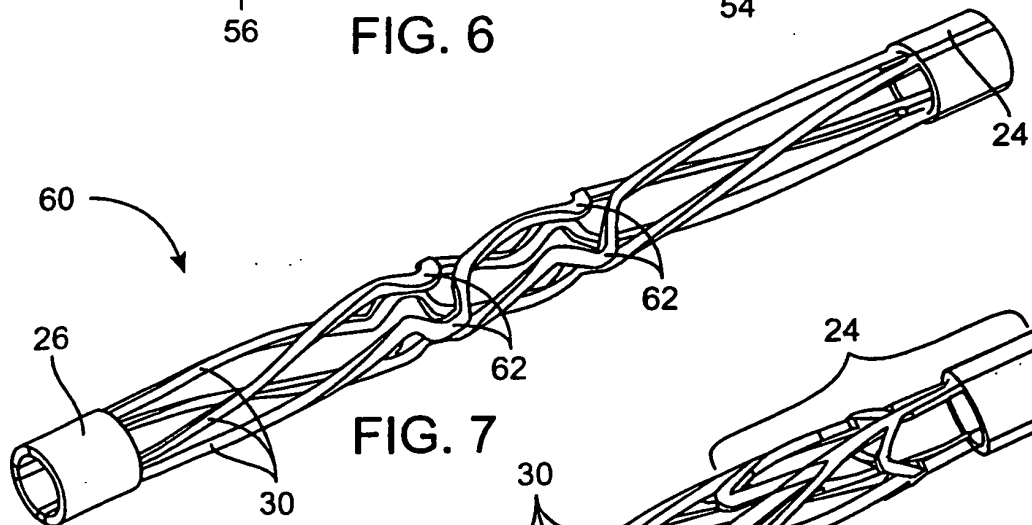
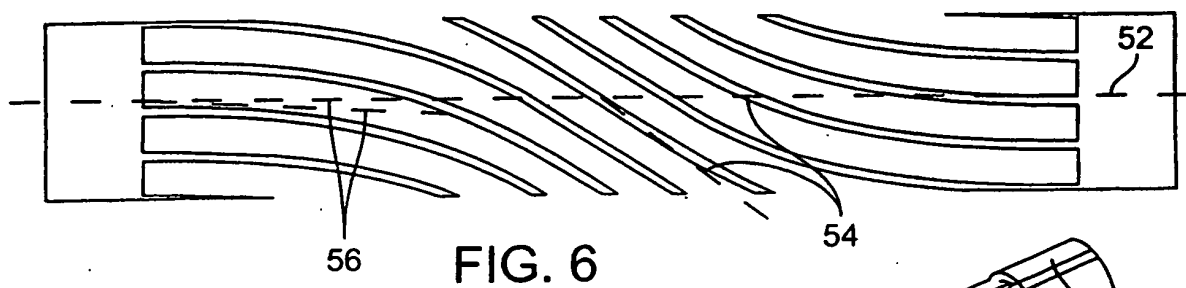
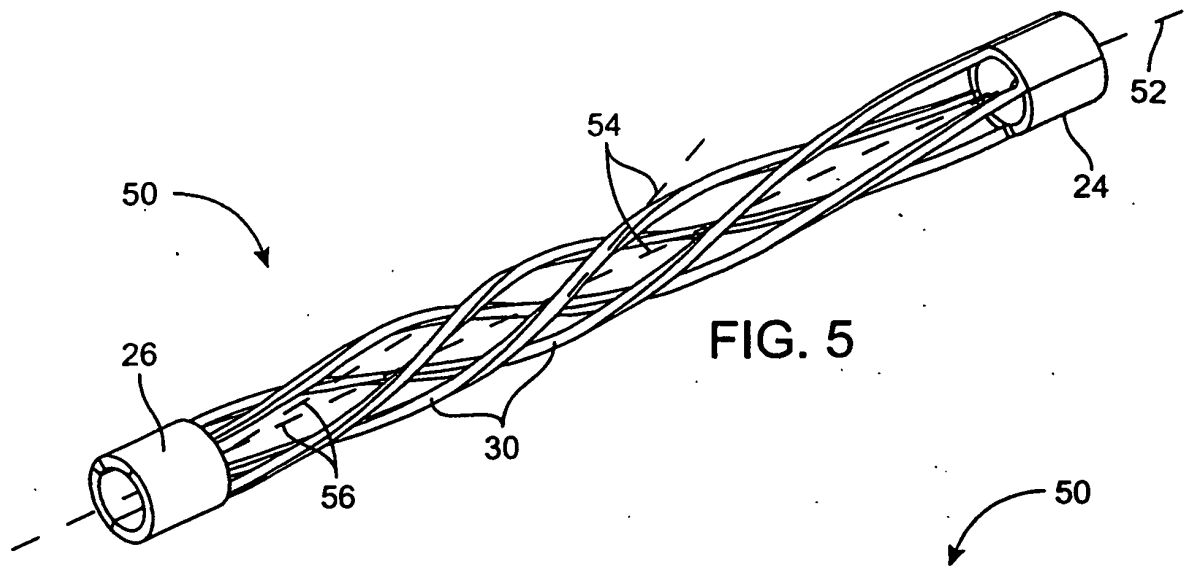
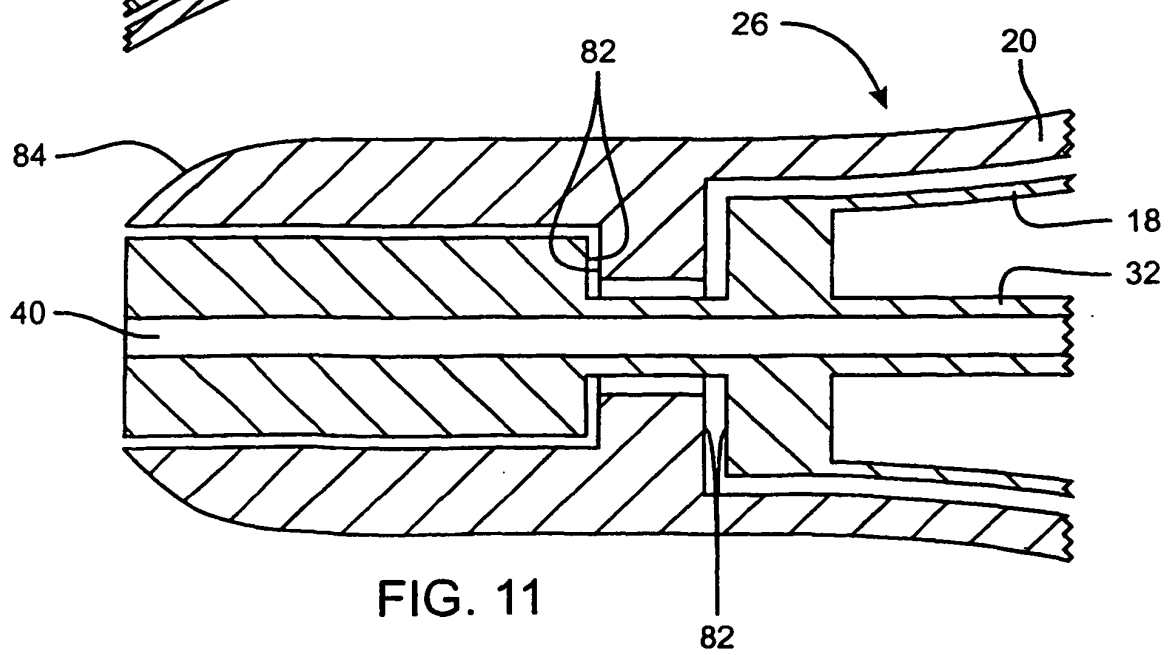
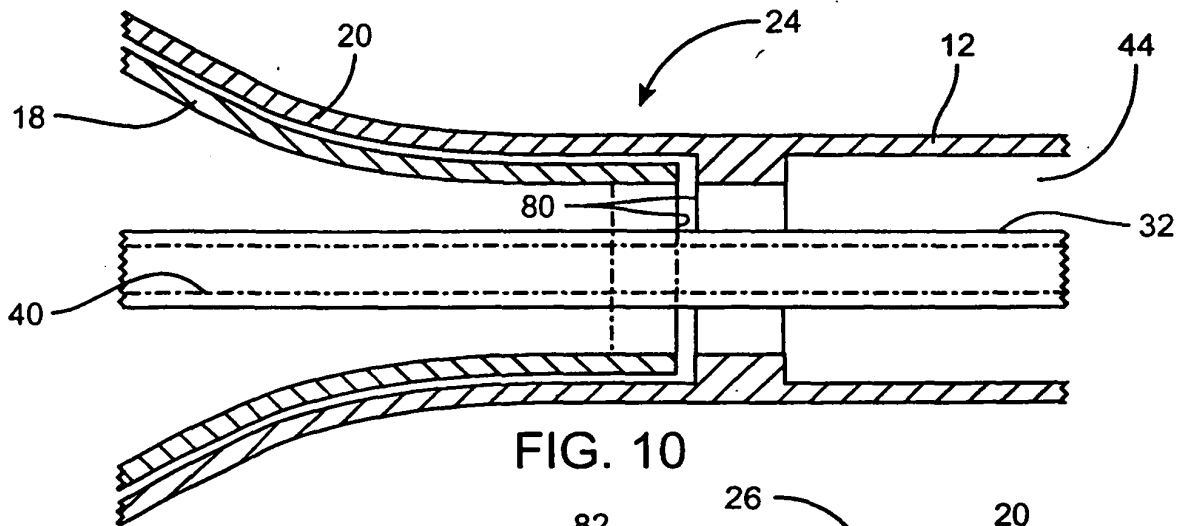
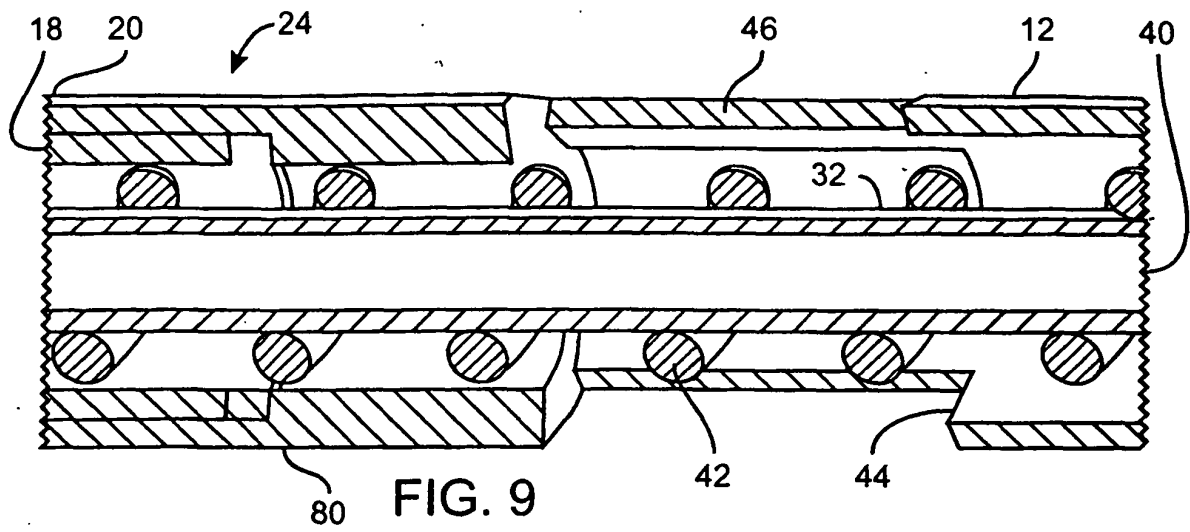
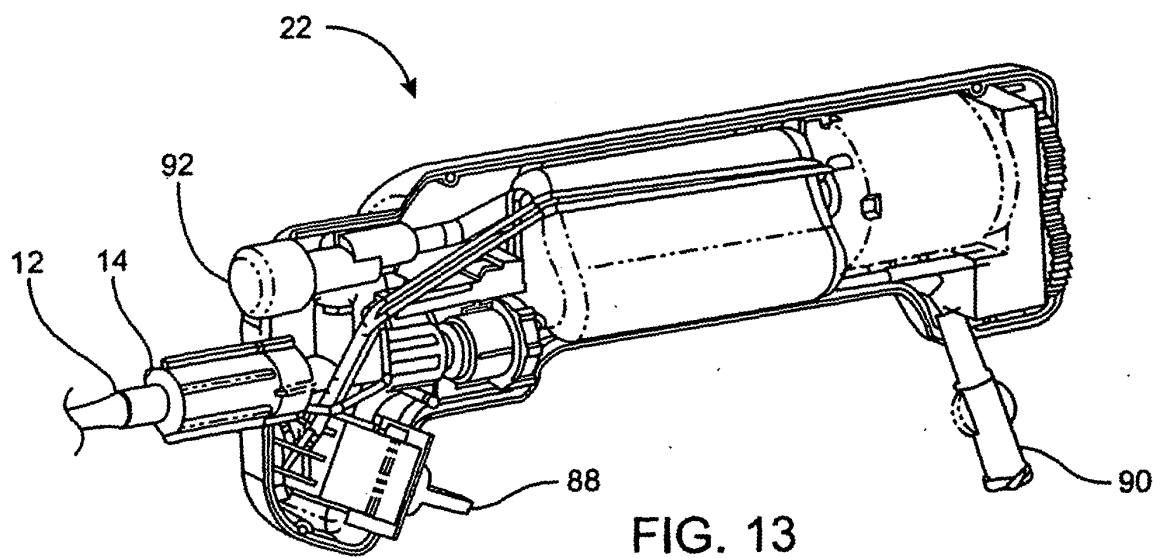
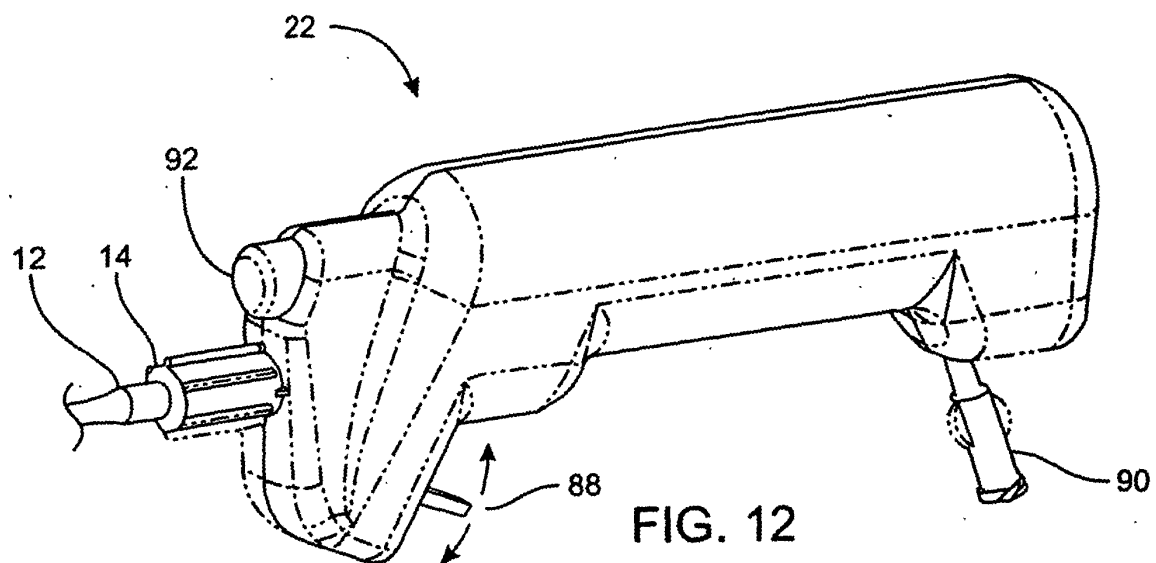
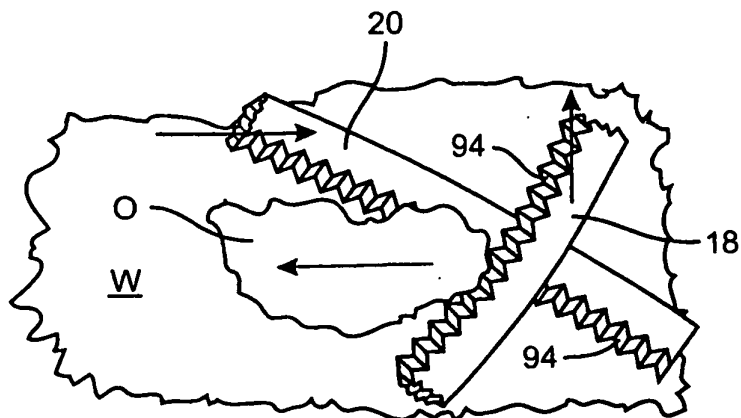
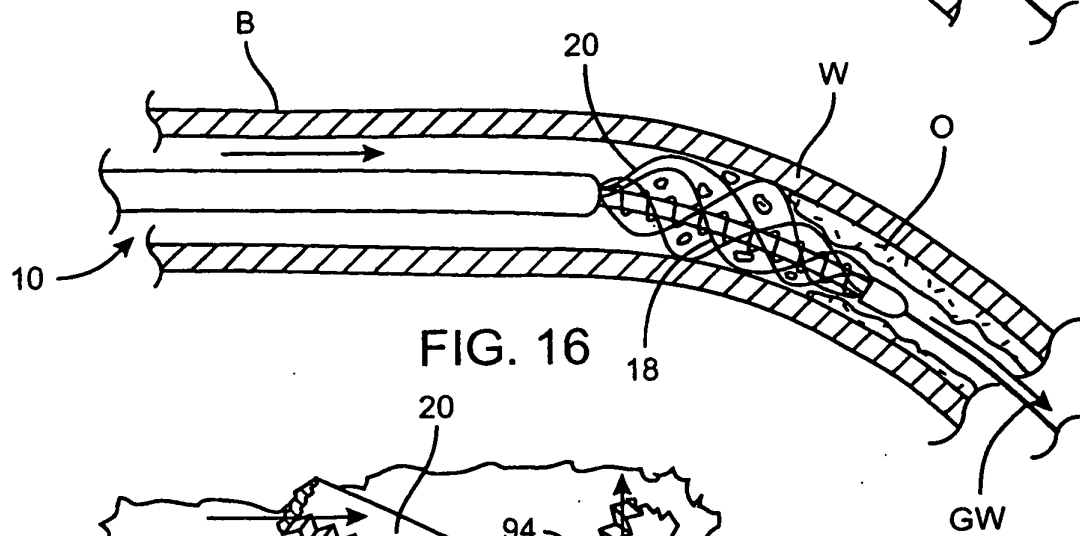
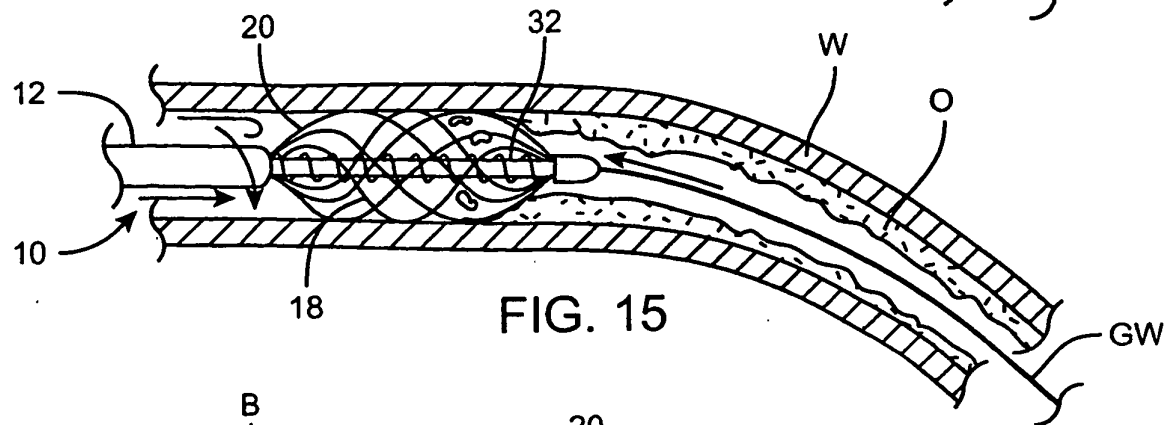
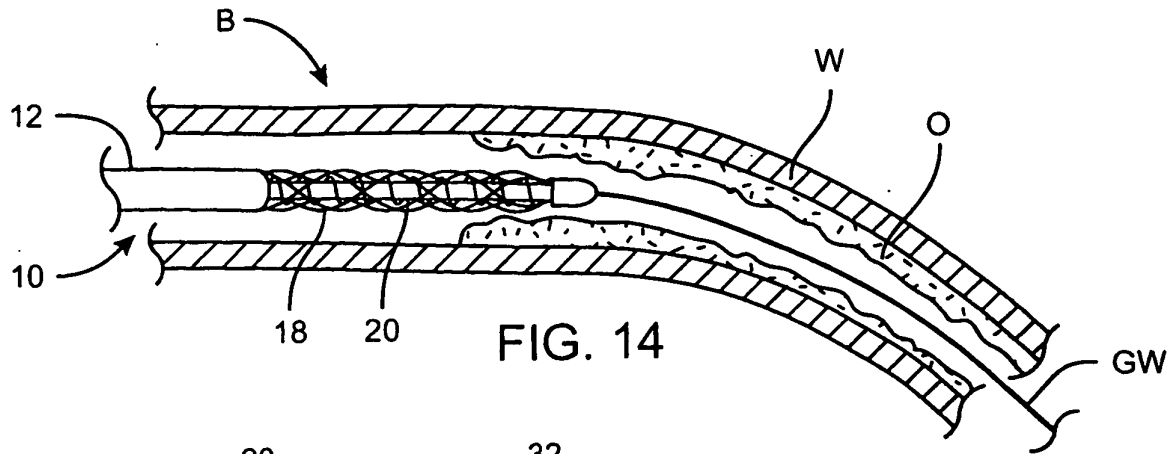


FIG. 3C









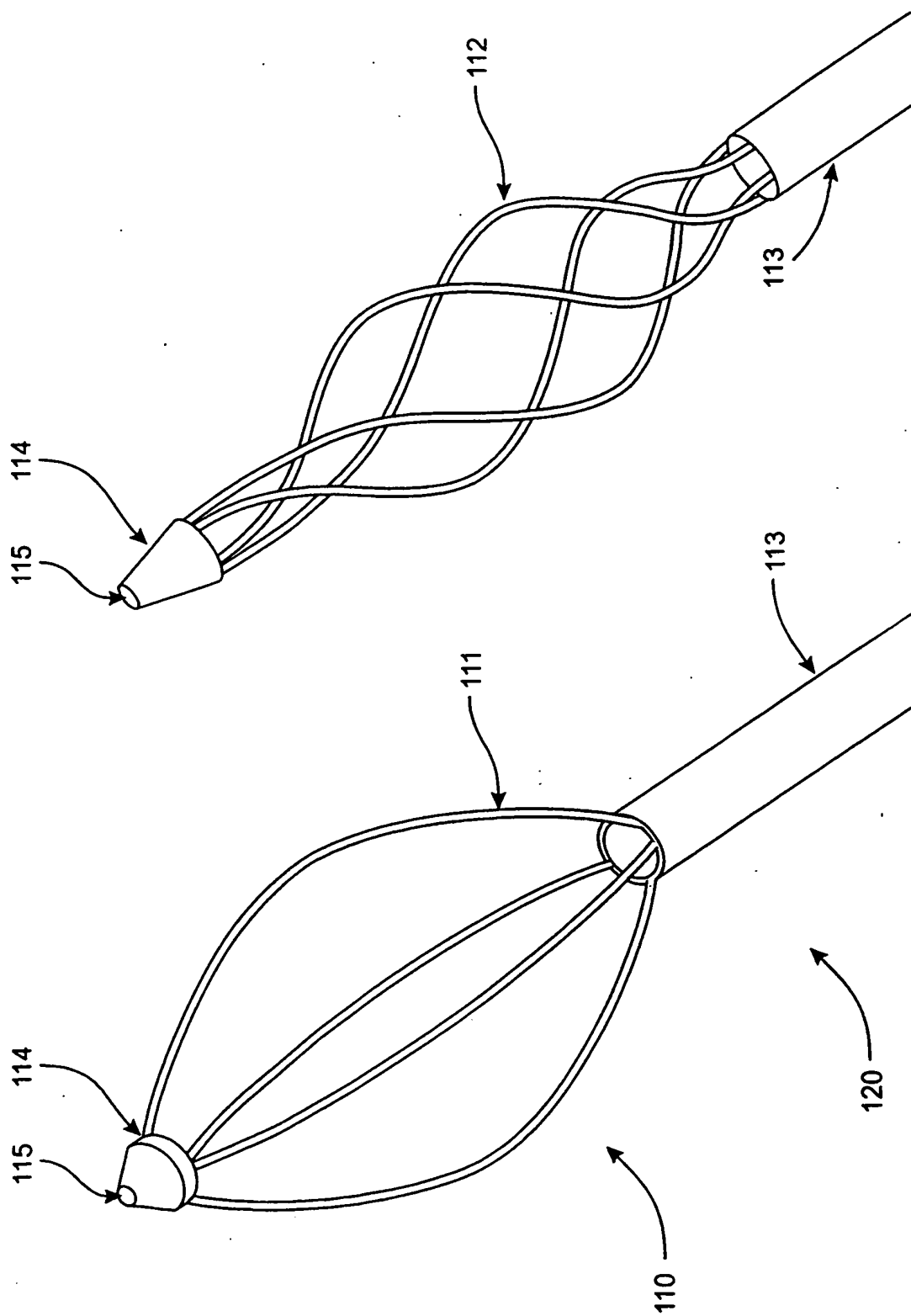


FIG. 18B

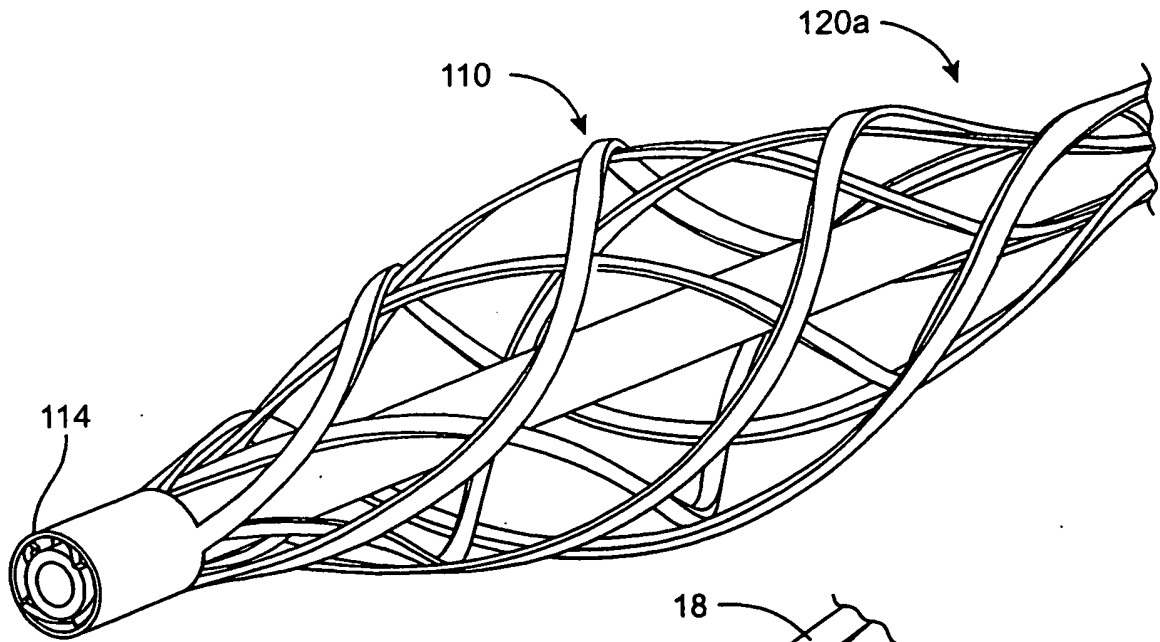


FIG. 18C

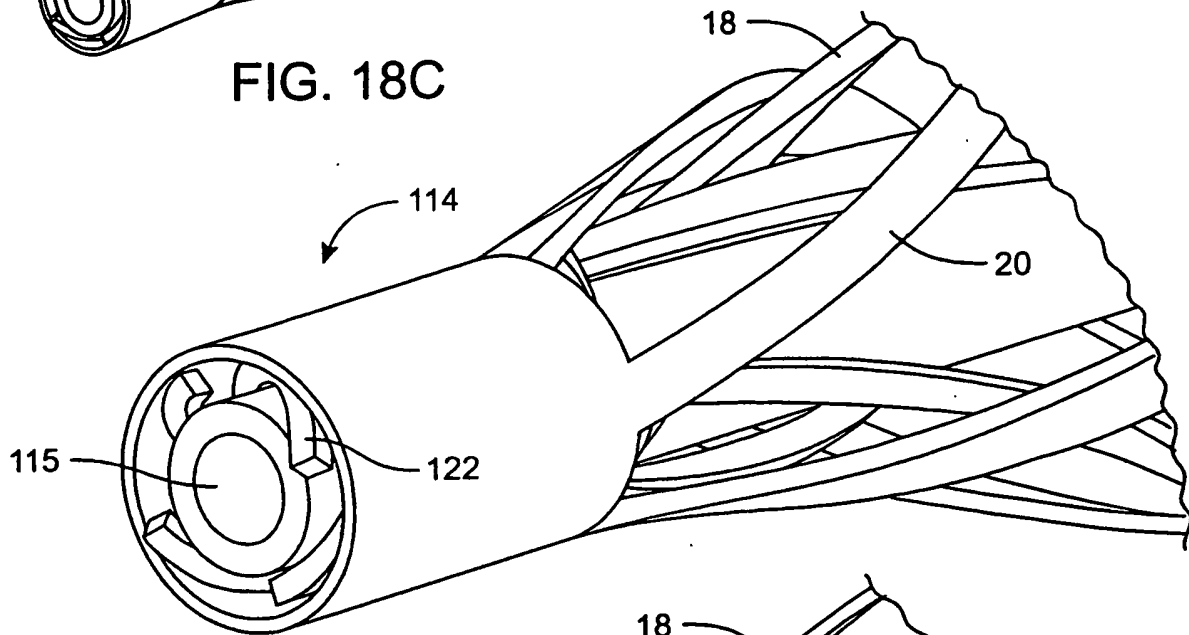


FIG. 18D

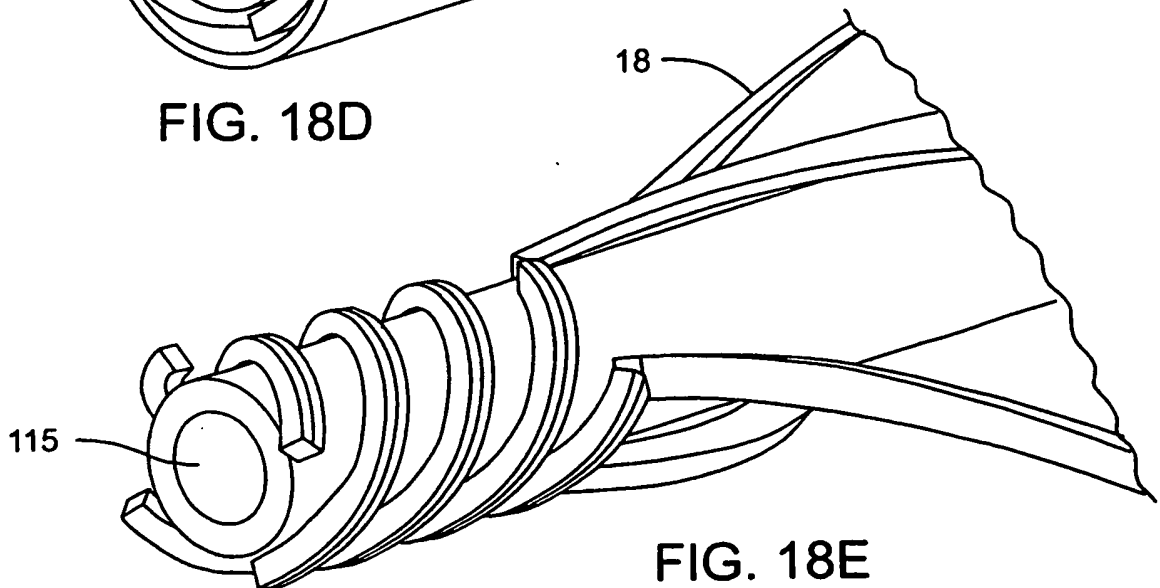


FIG. 18E

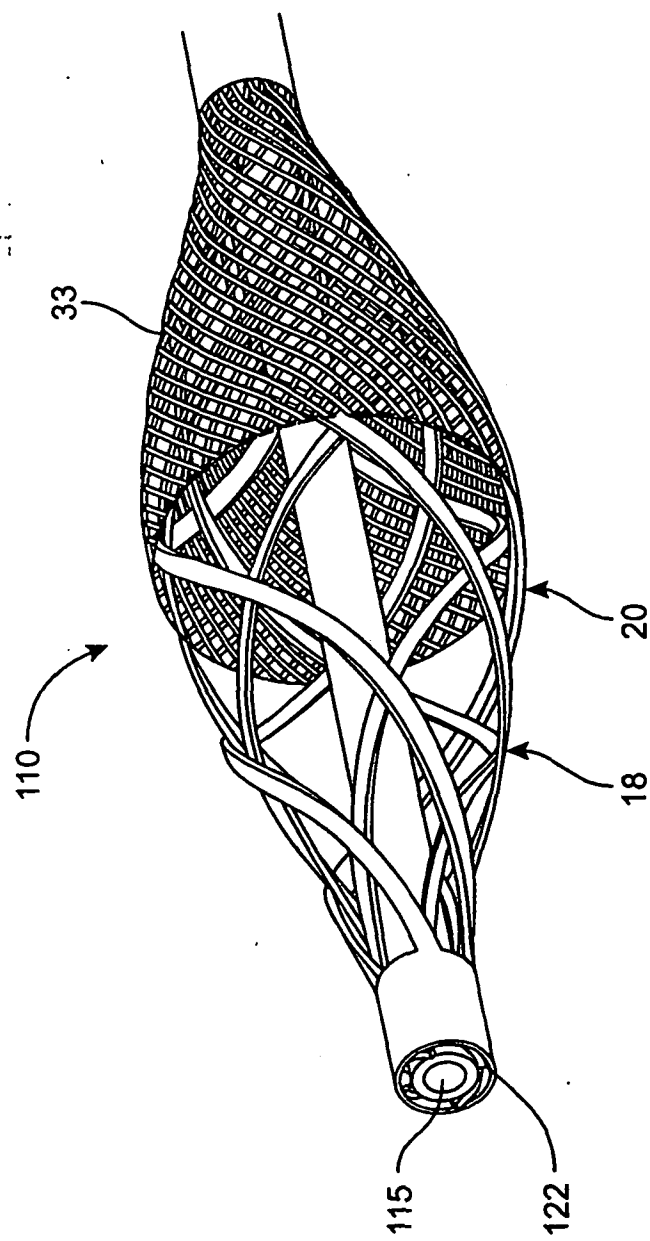


FIG. 18F

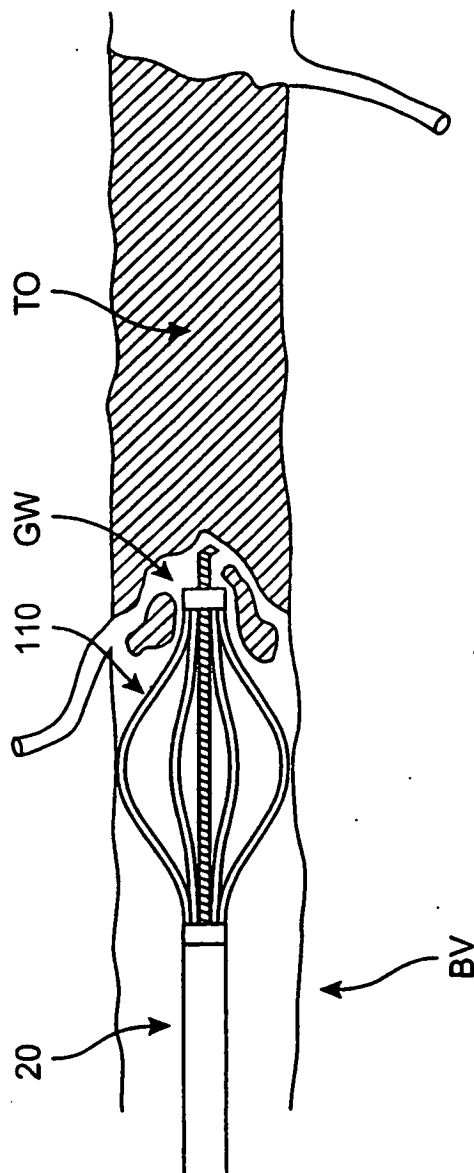
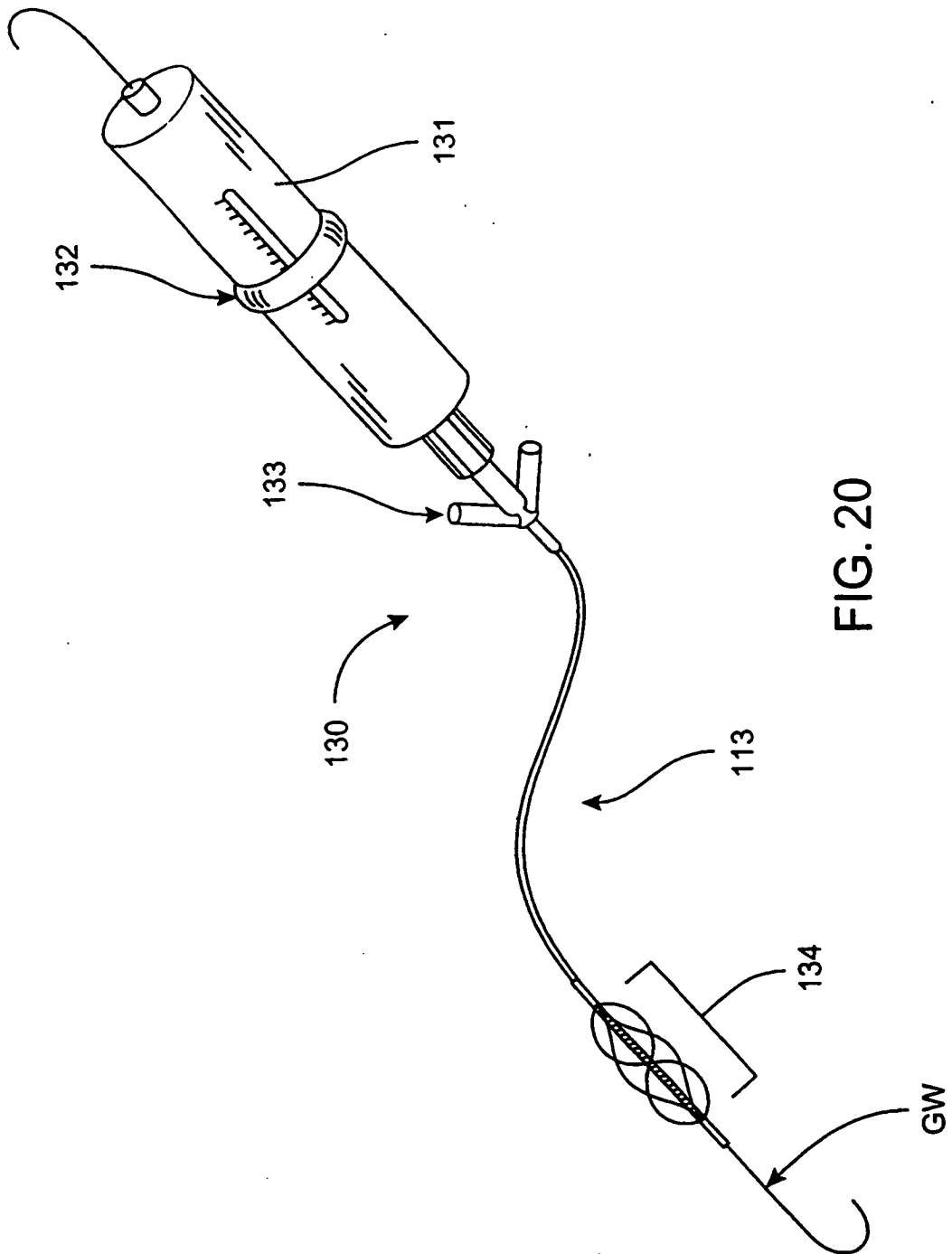


FIG. 19



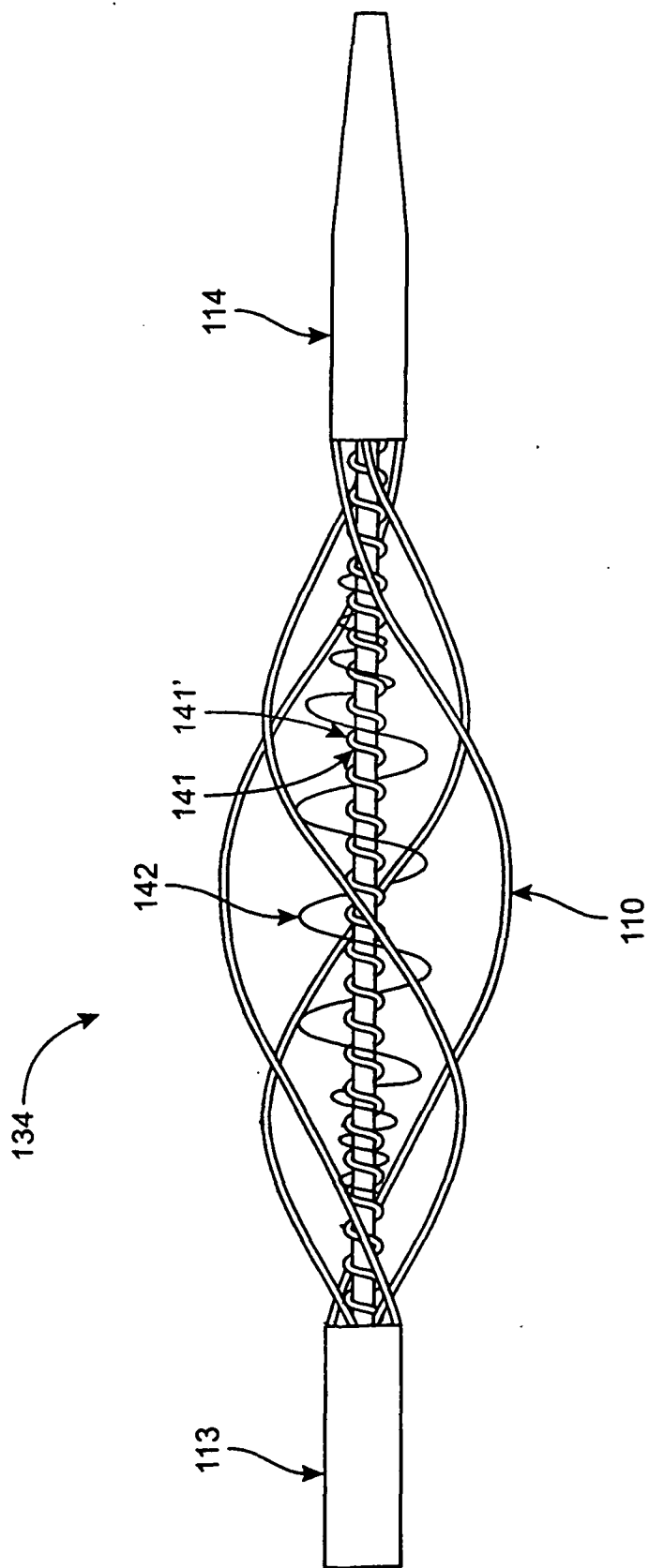


FIG. 21

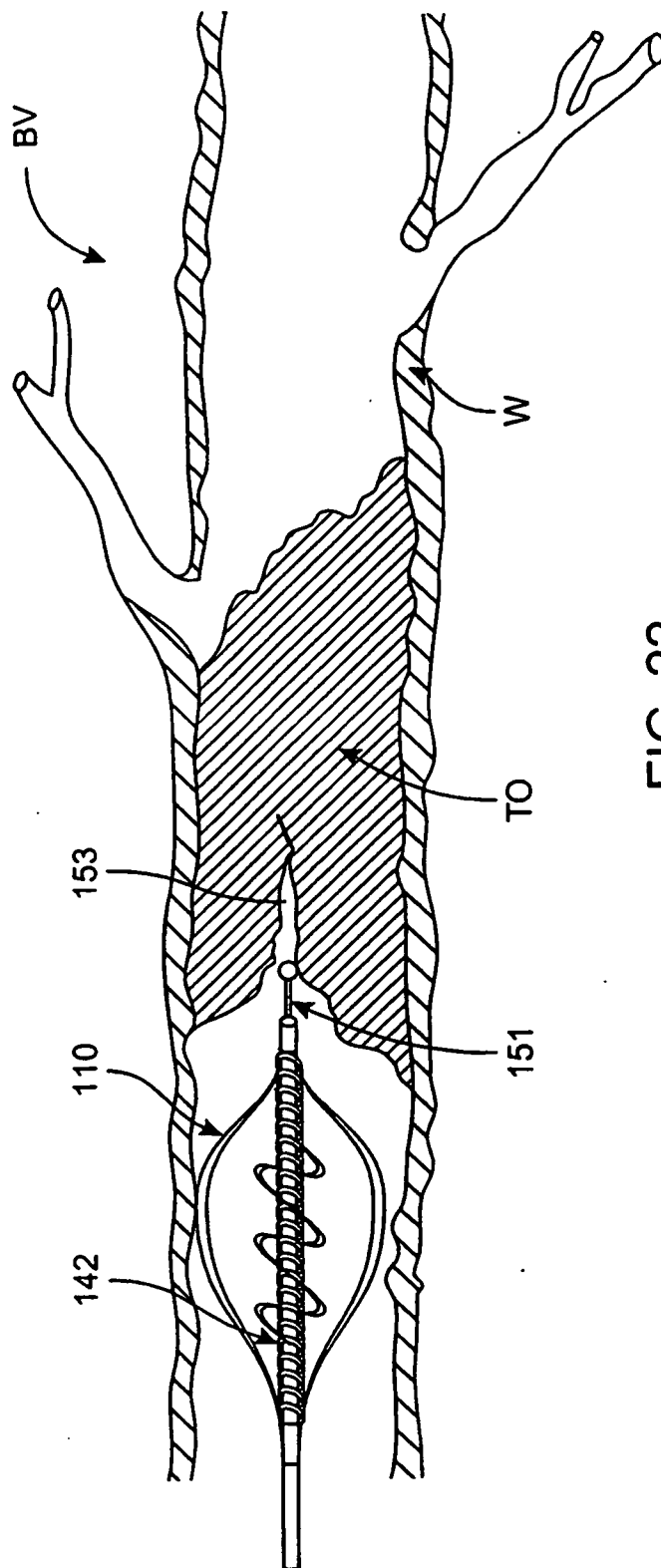


FIG. 22

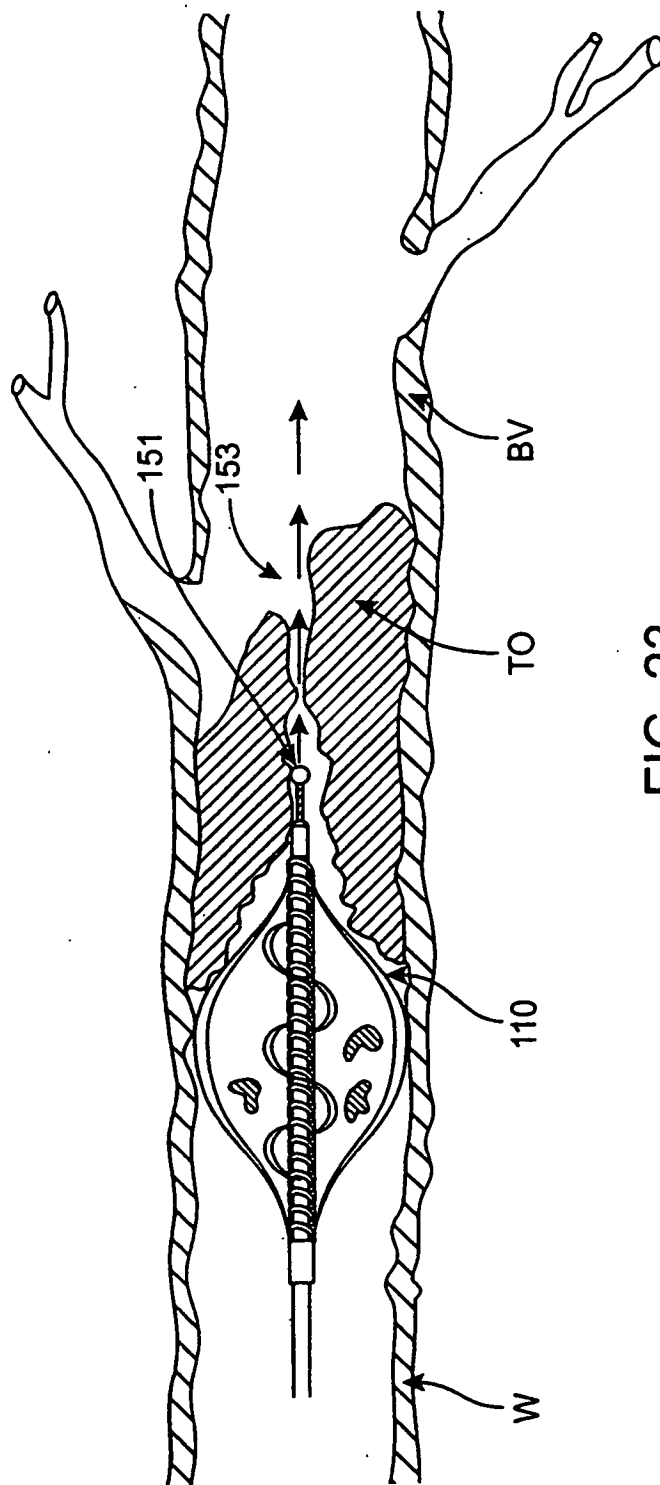
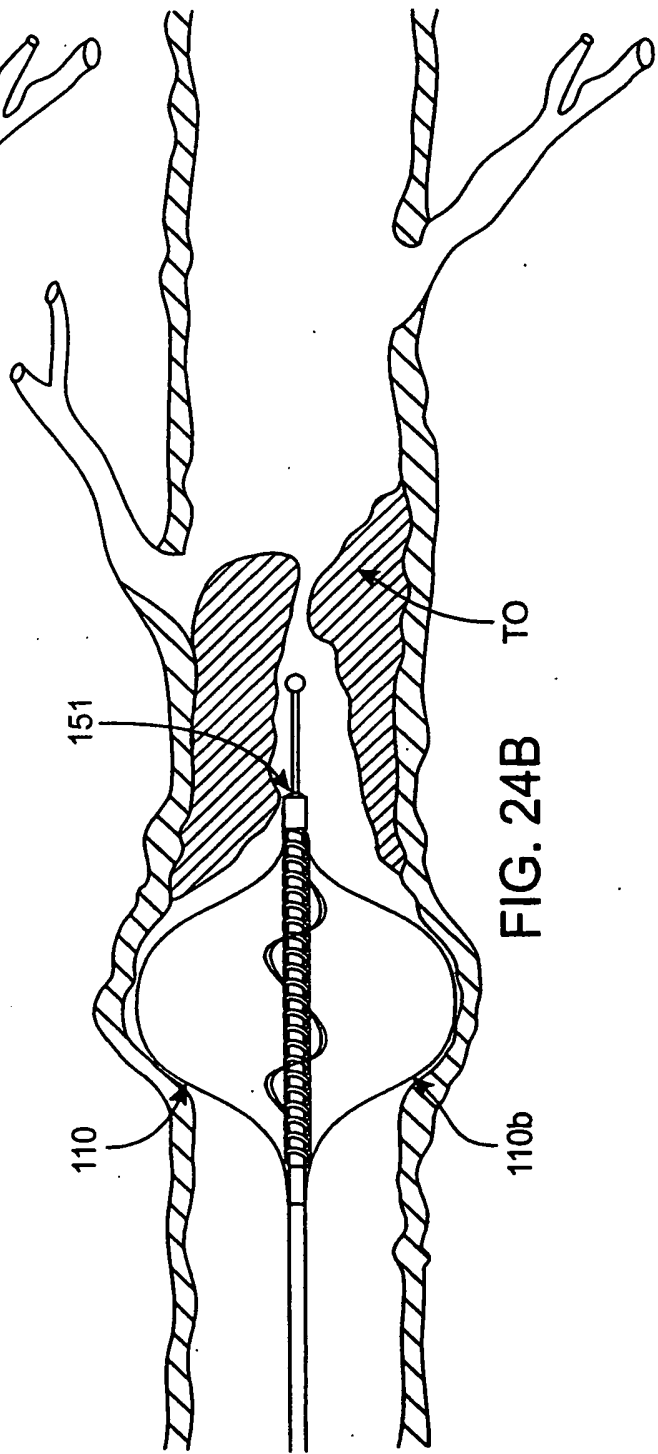
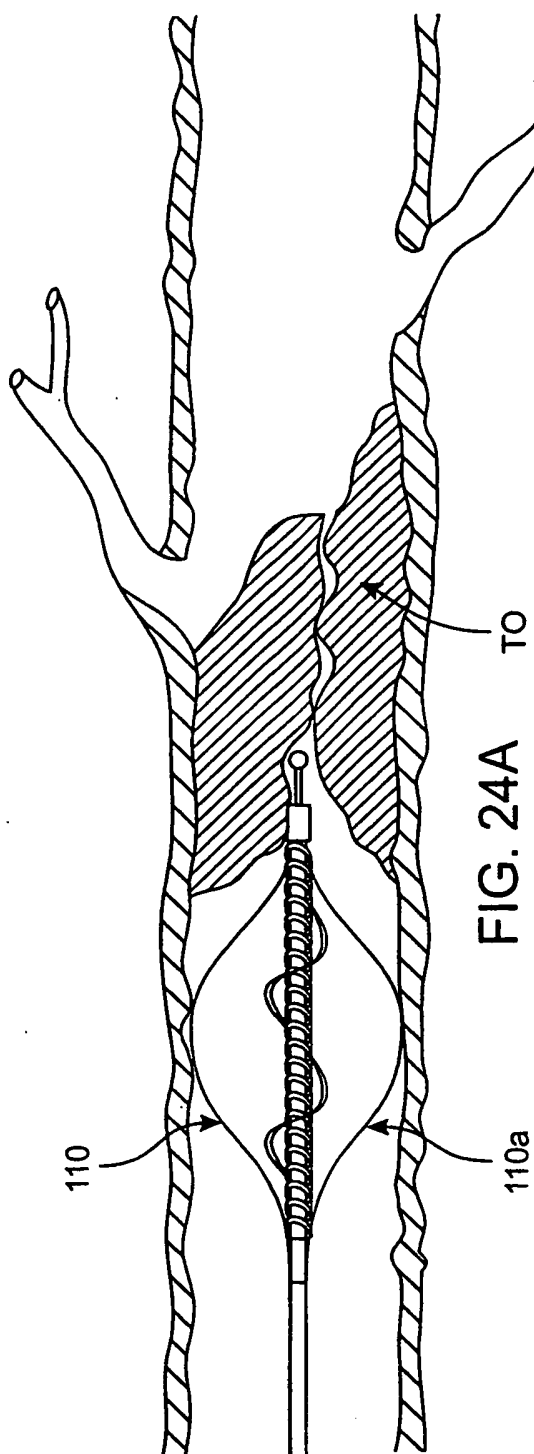


FIG. 23



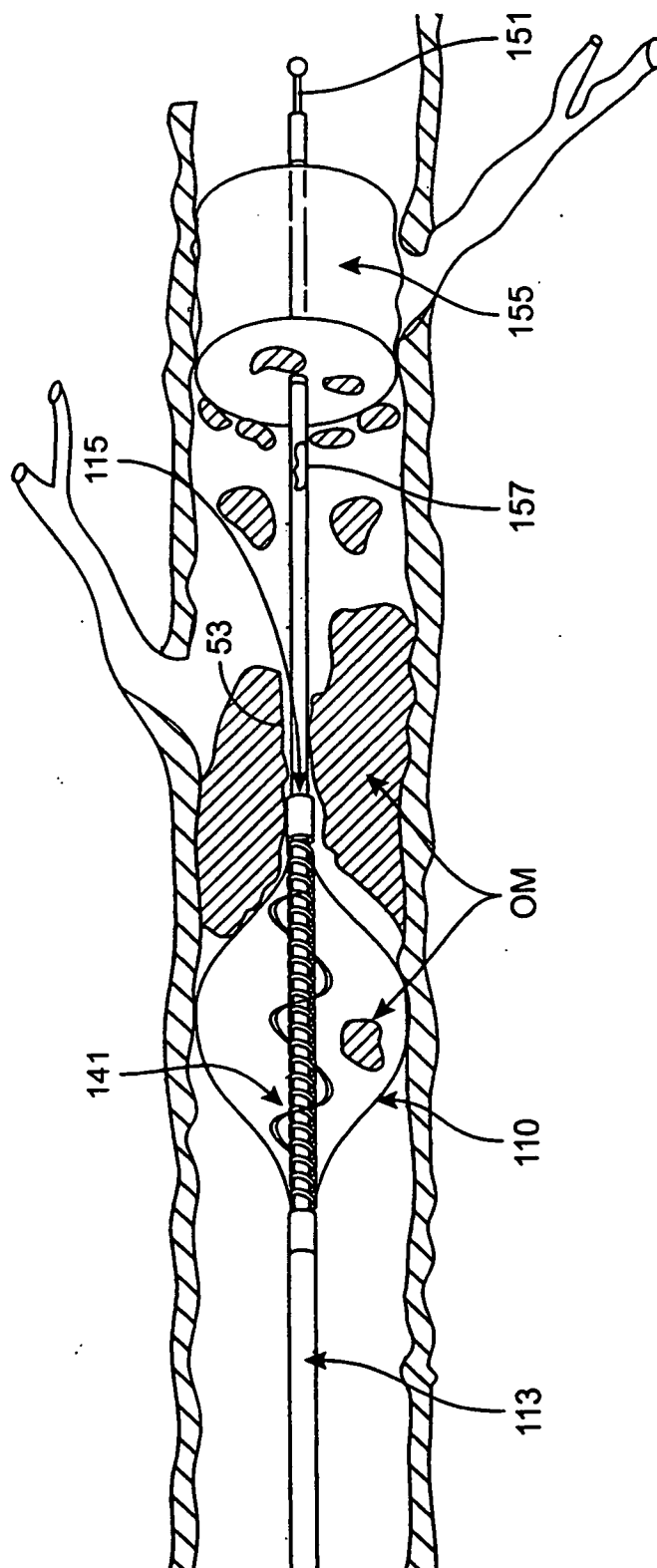


FIG. 25A

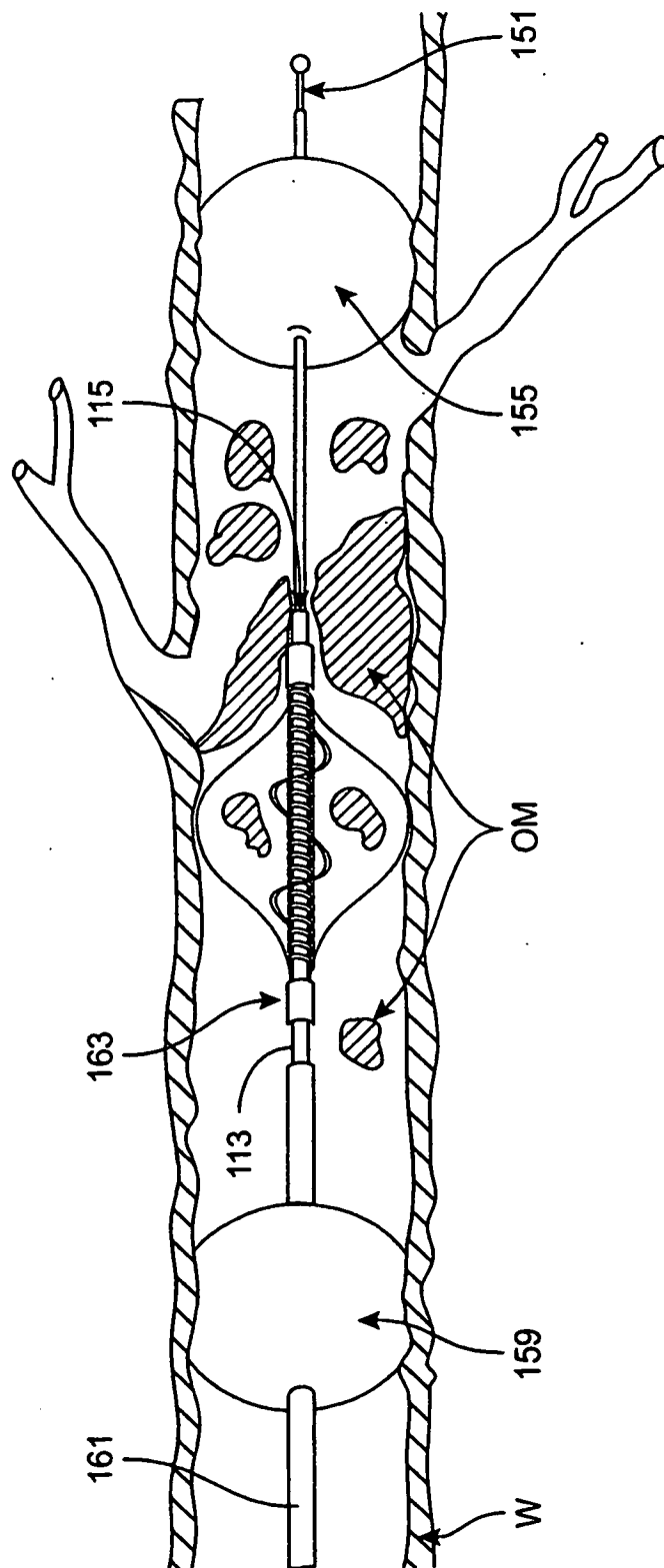


FIG. 25B

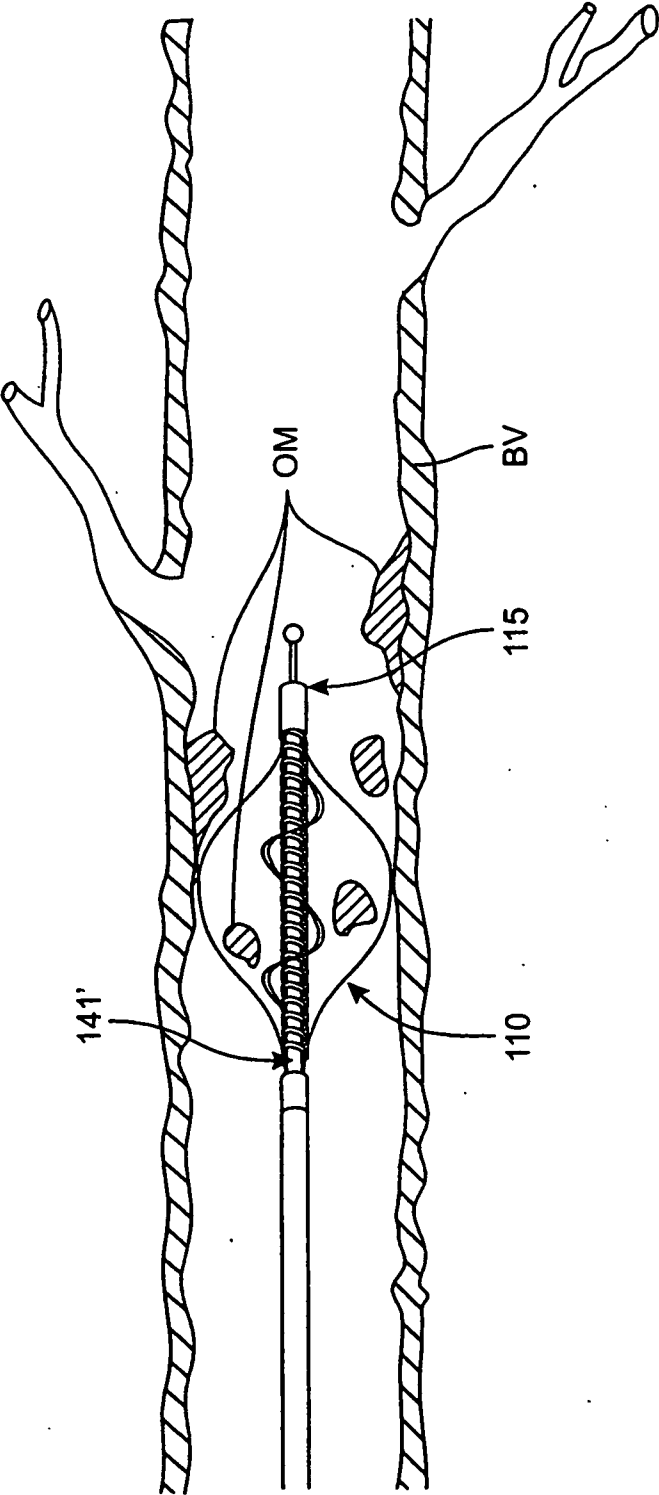


FIG. 25C

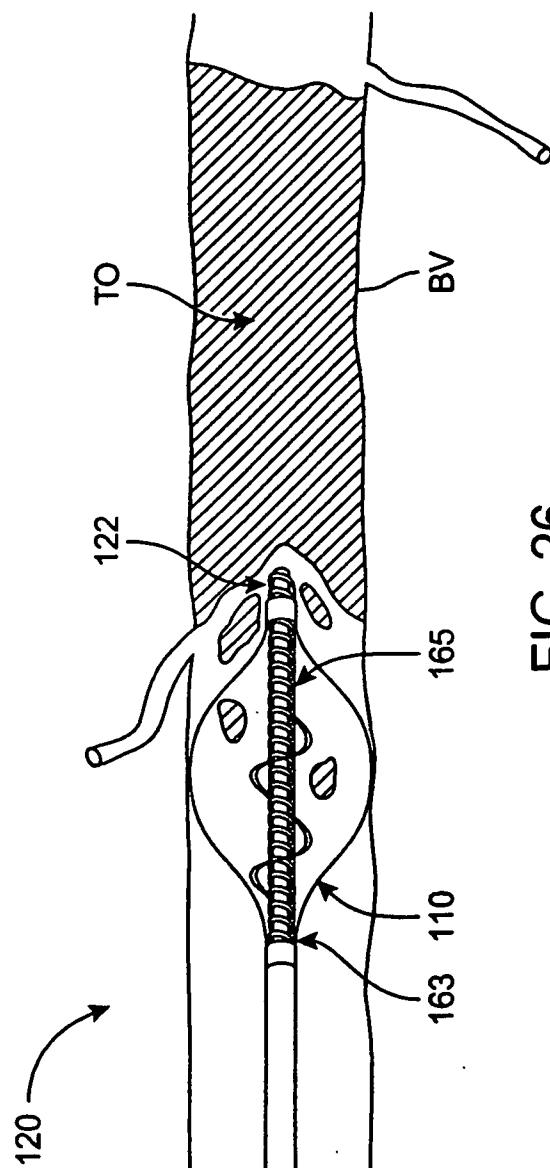


FIG. 26

REFERENCES CITED IN THE DESCRIPTION

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专利名称(译)	用于血栓和闭塞性材料去除的可扩张剪切导管		
公开(公告)号	EP1272110B1	公开(公告)日	2011-05-04
申请号	EP2001926502	申请日	2001-03-30
[标]申请(专利权)人(译)	血管BACCHUS		
申请(专利权)人(译)	BACCHUS血管INC.		
当前申请(专利权)人(译)	泰科医疗集团LP		
[标]发明人	LEEFLANG STEPHEN A DEMARAIS DENISE M EVANS MICHAEL A EVERSULL CHRISTIAN S		
发明人	LEEFLANG, STEPHEN, A. DEMARAIS, DENISE, M. EVANS, MICHAEL, A. EVERSULL, CHRISTIAN, S.		
IPC分类号	A61B17/22 A61B17/00 A61B19/00 A61F2/84 A61M25/00		
CPC分类号	A61B17/320725 A61B17/221 A61B17/320758 A61B17/320783 A61B2017/00685 A61B2017/22094 A61B2017/2212 A61B2090/08021		
优先权	60/193539 2000-03-31 US 60/260170 2001-01-04 US 09/820301 2001-03-27 US		
其他公开文献	EP1272110A4 EP1272110A1		
外部链接	Espacenet		

摘要(译)

装置，方法，试剂盒和方法从脉管系统和其他体腔中去除阻塞性物质。可膨胀的篮子可用作配合的径向可膨胀的剪切构件。每个篮子的螺旋定向支柱可以在均匀的圆周方向上卷绕。支柱可以是独立的柔性，允许剪切构件轴向一起弯曲。内篮可以被可旋转地驱动，并且可以使用从剪切构件和/或远侧穿透器向近侧延伸的轴向泵，用于推进阻塞导丝进入的闭塞。支柱可以基本上连续地彼此滑动，并且对于高效血栓切除术可以具有足够的侵略性。旋转静止且轴向柔性的外篮可提供安全的，有限的粥样斑块切除术治疗。

