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(57)

ABSTRACT

The invention relates to an electrosurgical instrument (10) comprising two limbs (15, 16) that have an articulated connection and that can be actuated in the manner of a cutting or clamping tool. The instrument also comprises opposing electrode parts (22, 23) with coagulation surfaces (22a, 23a) on distal ends (11, 12) of its limbs for holding a vessel or tissue and for passing a current through said vessel or tissue to coagulate the latter, wherein at least one electrode part has an open region (22d, 23d) that acts as a guide gap (24) for a cutting instrument (30), so that the electrode part(s) is/are divided into at least two areas and the cutting instrument can be placed on the held vessel or tissue to execute a cutting operation. In addition, current supply devices (20, 21) supply the coagulation current from a high-frequency generator to the electrode parts. The improved configuration of said electrosurgical instrument allows the open region on the electrode part(s) to afford optimal guidance of a cutting instrument, whereby said open region can be easily prepared for additional cutting operations and/or subjected to an after-treatment. To achieve this, the two or more open regions of the electrode part(s) comprise respective opposing separation surfaces (22e, 22e', 23e, 23e') that taper towards the coagulation surfaces.

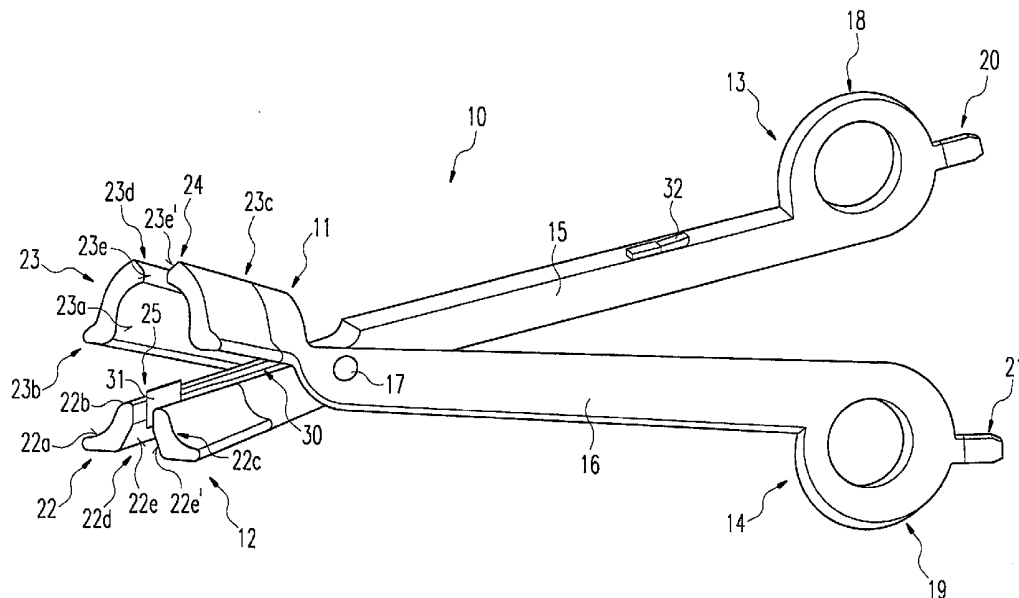
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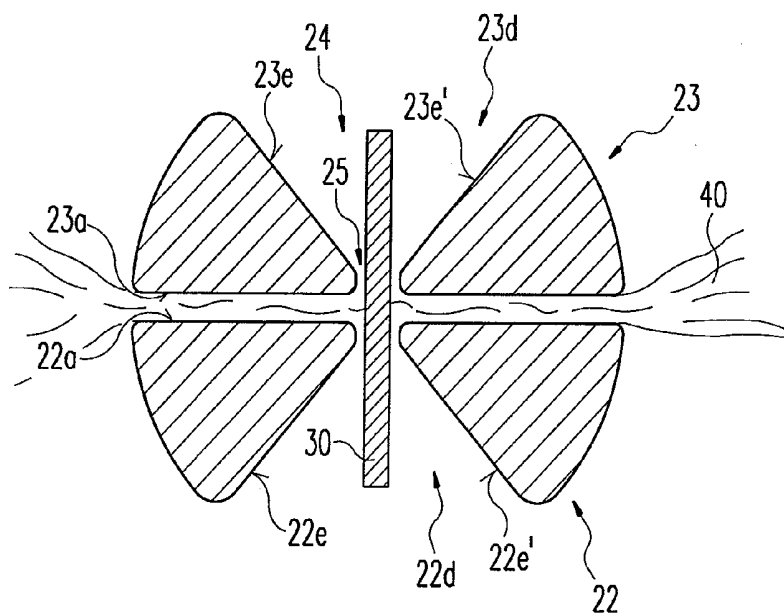


Fig. 1

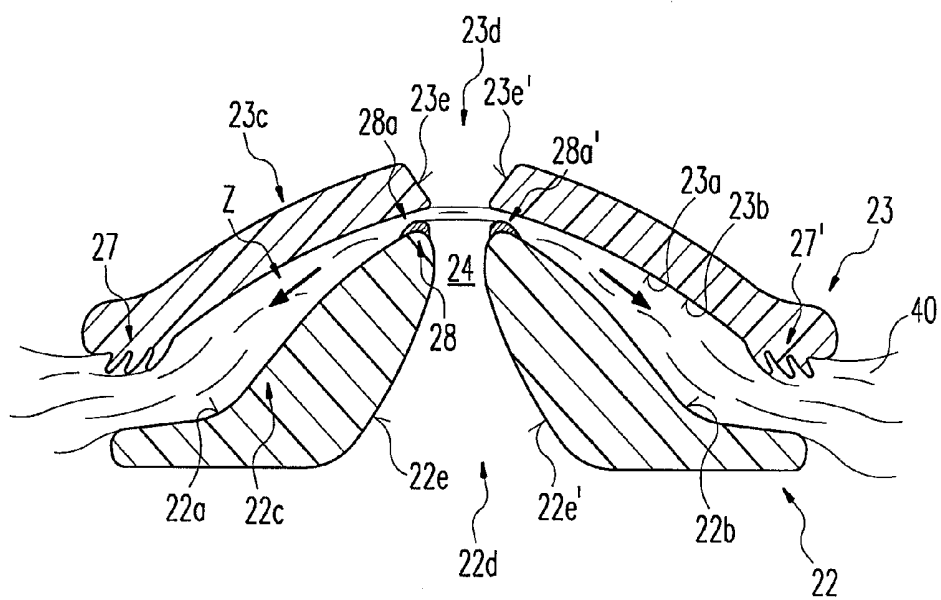
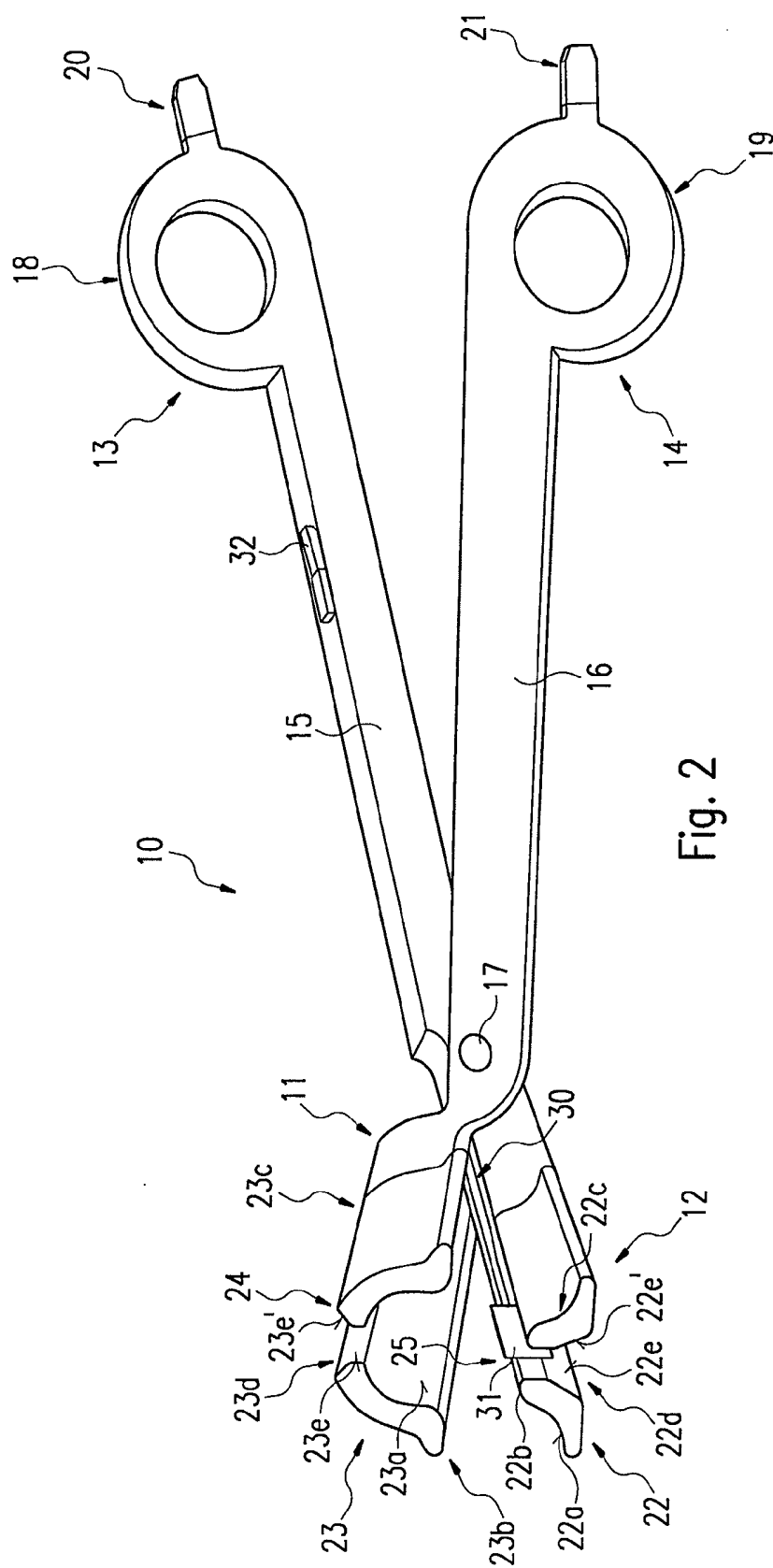


Fig. 5



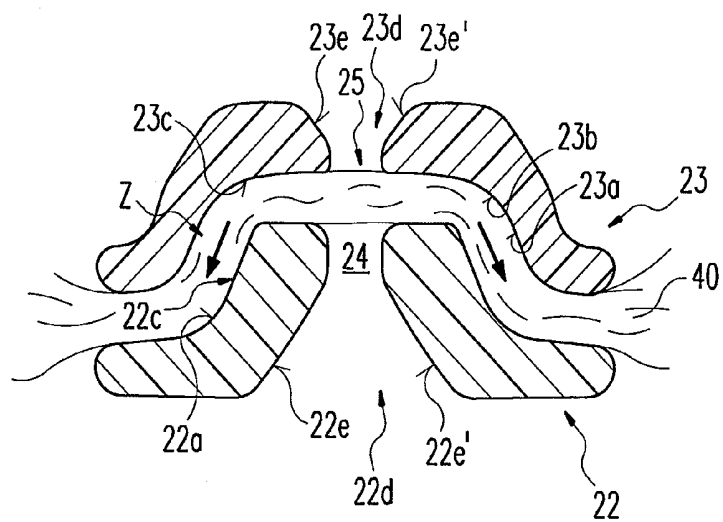


Fig. 3

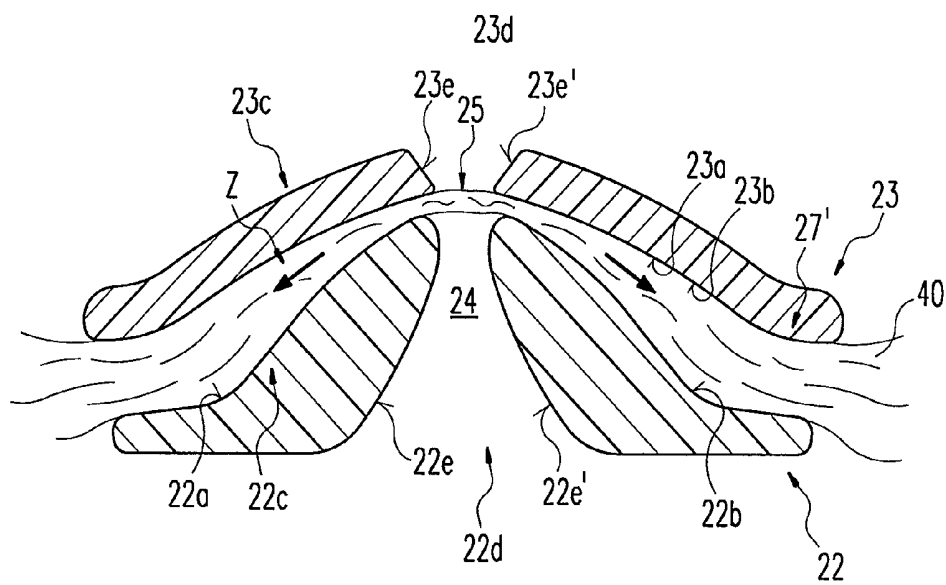


Fig. 4

ELECTROSURGICAL INSTRUMENT

RELATED U.S. APPLICATIONS

[0001] Not applicable.

STATEMENT REGARDING FEDERALLY
SPONSORED RESEARCH OR DEVELOPMENT

[0002] Not applicable.

REFERENCE TO MICROFICHE APPENDIX

[0003] Not applicable.

FIELD OF THE INVENTION

[0004] The invention relates to an electrosurgical instrument according to the preamble of claim 1.

BACKGROUND OF THE INVENTION

[0005] Electrosurgical instruments have been used for many years in high-frequency surgery especially in order to coagulate biological tissue as well as to cut it. For coagulation a high-frequency current is passed through the tissue to be treated, so that it changes due to protein coagulation and dehydration. The tissue contracts in such a way that the vessels are closed and bleeding is staunched. After coagulation has taken effect the tissue can, for example, be separated by means of a mechanically operating cutting instrument.

[0006] Electrosurgical procedures can be carried out in a monopolar as well as a bipolar way. With monopolar technology the electrosurgical instrument has only one current supply and the tissue to be treated (or the patient) must therefore be placed at the other potential. Bipolar instruments which are constructed with two separately isolated sections are gaining more and more in significance, however. The current path between the electrode parts can thus be calculated and does not run long distances through the body of the patient. The effect of, for example, pacemakers or other equipment which are connected to the patient during an operation is thus reduced.

[0007] Bipolar coagulation instruments comprise essentially two limbs that have an articulated connection at whose proximal ends handle devices are provided for handling the limbs. At the distal ends of the limbs are electrode parts with coagulation surfaces for gripping the tissue and for passing the coagulation current through the tissue. For this the HF current supplied by a HF generator is fed via current supply devices to the electrode parts of the bipolar instrument.

[0008] Known bipolar coagulation instruments often comprise open regions on the electrode parts forming a guide gap for a cutting instrument. This means that the electrode parts are at least partially divided, so that cutting instrument can be placed on the tissue clamped between the electrode parts. The guide gap therefore facilitates access for the cutting instrument to the tissue while being held between the electrode parts of the coagulation instrument. Also, the guide gap is provided to guide the cutting instrument in order to guarantee precise cutting of the tissue. This is advantageous particularly for mechanically operated cutting instruments.

[0009] Such an instrument is, for example, known from US 2003/0229344 A1. Bipolar tongs are shown where the

effector unit and in particular its electrically conductive areas comprise slits to facilitate access for a cutting instrument to the tissue clamped in the effector unit. The slits are constructed in such a way that the coagulation surfaces of the electrode parts are disrupted as little as possible. With this embodiment of the slits their preparation for reuse, that is to say cleaning, is very time-consuming as the access into the slits is made difficult.

[0010] In order to counteract this problem a very wide slit or guide gap is provided in other known instruments. Here a considerable reduction in the coagulation surfaces or insufficient guidance of mechanical cutting instruments in particular has to be accepted.

[0011] Known instruments are also provided as disposable instruments in order to save cleaning. This has considerable cost implications.

BRIEF SUMMARY OF THE INVENTION

[0012] The object of the invention therefore is to further develop an electrosurgical instrument for coagulation of the above-mentioned type in such a way that an open region is guaranteed permanently on least at one electrode part for optimum guidance of a cutting instrument.

[0013] This object is achieved by an electrosurgical instrument according to claim 1.

[0014] The object is achieved in particular by an electrosurgical instrument which comprises two limbs that have an articulated connection which can be actuated corresponding to a cutting or clamping tool. The instrument comprises further electrode parts positioned opposite each other with coagulation surfaces at distal ends of the limbs for gripping a vessel or tissue and for passing a coagulation current through the vessel or tissue for its coagulation, wherein at least one electrode part comprises an open region as a guide gap for a cutting instrument, so that at least one electrode part is divided into two areas and the cutting instrument can be applied to the vessel or tissue held in order to carry out a cutting procedure. Moreover, current supply devices are provided for passing the coagulation current from a HF generator to the electrode parts. The at least two areas of the at least one electrode part comprise respective separation surfaces arranged opposite each other tapering in the direction of the coagulation surfaces.

[0015] An essential point of the invention is that the guide gap expands in the direction which faces away from a cutting area between the electrode parts on both electrode parts. Precise guidance of the cutting instrument is thus possible in direct proximity to the cutting area based on the tapered construction of the guide gap and the coagulation zone of the electrode parts is hardly disrupted. The other areas of the guide gap are at the same time easily accessible and thus easy to clean. If the guide gap has to be re-worked, for example a coating having to be applied, then this can be carried out easily because of the improved access.

[0016] In a preferred first embodiment the open regions are provided at the opposite electrode parts wherein these are essentially aligned when the limbs are brought together. If only one open region has been formed at one electrode part this is especially suitable for cutting tissue with, for example, a surgical knife, wherein the tissue rests completely on the opposite electrode part in a tensioned state. If

open regions are provided at both electrode parts surgical scissors can, for example, be used on the coagulated tissue and this is easily cut. In order that a well-calculated cut can be carried out the open regions are preferably arranged in the central sections of the electrode parts.

[0017] In a further preferred embodiment the cutting instrument is combined with the electrosurgical instrument. The cutting instrument is, for example, situated within one of the limbs and can be brought into a cutting position when required. A change of instruments is thus avoidable, so that the course of an operation does not have to be disrupted.

[0018] With the cutting instrument integrated in the coagulation instrument both electrode parts are preferably constructed with the open region, so that the cutting instrument can reach the tissue unhindered.

[0019] If the cutting instrument is not constructed so that it is integrated with the electrosurgical instrument, the guide gap has then to be arranged in such a way that a cutting instrument introduced from the outside can be placed with sufficient accuracy at the pretensioned tissue.

[0020] One advantageous embodiment provides for the cutting instrument being mechanically and/or electrically operated. A blade constructed on a shaft on the electrosurgical instrument can, for example, be provided which is housed in the limb during coagulation and is applied to the tissue for the cutting procedure. Positioning of the blade or another cutting instrument and also feeding it forward can occur automatically or be carried out by the surgeon mechanically.

[0021] A solution according to the invention provides for the cutting instrument being constructed for cutting by means of a HF-current and for being connected to a control unit, so that the cutting current supply depends on the operation phases. The surgeon can control the cutting procedure so that it runs automatically and is optimised.

[0022] In a preferred embodiment it is provided that the electrode parts comprise at least one tensioning area each in such a way that when clamping the tissue it is pretensioned between the electrode parts and the cutting procedure can be carried out on the pretensioned tissue by means of the cutting instrument. The tissue under tension is then easier to cut by means of the cutting instrument in particular by means of a mechanical cutting instrument, as tissue fibres are aligned at right angles to the cutting direction and the tissue becomes thinner in the procedure. The force needed to completely cut pretensioned tissue is thus considerably reduced and mechanical stress on the cutting instrument, in particular wear of cutting sections, is counteracted. The cutting procedure itself is also easier for the surgeon and the instrument is easier to handle. As a result of the separation surfaces of the electrode parts tapering towards the cutting area a mechanically operated cutting instrument in particular can be applied easily at the guide gap.

[0023] In a preferred embodiment one of the tensioning areas has a convex curvature at least in a first central section while the tensioning area positioned opposite has a concave curvature at least have essentially a positive fit. As a result of the curved tensioning areas tensioning of the tissue is facilitated in the simplest way because it is pulled, that is to say stretched, by the curved areas on both sides in the

direction of their end areas. Because of the tight fit the tissue tensioned between the limbs is securely held in a tensioned state.

[0024] The terms "convex" and "concave" in this context are not just to be understood as a rounded arc. These terms rather mean any kind of elevation or recess, hence also a roof-like elevation and thus a V-shaped recess.

[0025] In a further preferred embodiment one of the tensioning areas has a convex curvature at least in a first central section while the tensioning area positioned opposite has a concave curvature at least in the second central section. A radius of curvature of the concave tensioning area at least in the second central section is greater than a radius of curvature of the convex tensioning area in the first central section. The curvatures run along the longitudinal axes of the distal ends in such a way that the vessel or tissue that is held between the distal ends and extends perpendicularly to the longitudinal axes is held with a pressure that increases towards the first and second central sections. Based on the different curvatures of the coagulation surfaces contact between the coagulation surfaces can, seen mathematically, only occur at their crests. This means that an area of maximal proximity is formed between the coagulation surfaces that extends symmetrically around the crests of the coagulation surfaces. In this area tissue is particularly strongly pressed together as a result of the limbs being brought together due to the increased pressure compared to the other coagulation areas and is thus safely held between the electrode parts.

[0026] It is advantageous that the smooth geometry is easy to produce, inhibits adherence of tissue during the procedure and the coagulation surfaces can be easily prepared for reuse and if required reconditioned. In addition secure closure of a vessel or tissue is achieved as a result of the high clamping force in the area of high pressure.

[0027] In one of the solutions according to the invention it is provided that at one tensioning area and/or on the opposite tensioning area a surface profile is formed which supports the tensioning effect. The profile is preferably formed at the end areas of the respective tensionings and moves the tissue additionally in a direction of pull defined by the tensioning areas or prevents a backward movement of the tissue against this direction of pull.

[0028] The surface profile supporting the tensioning effect is preferably constructed as a saw tooth profile. The teeth of the profile can, for example, be arranged in such a way that during the bringing together of the limbs they increasingly grip the tissue and transport it in the direction of pull. This increases the tension in the tissue considerably. Care must, however, be taken that injury to the tissue caused by the profile is avoided, so that the teeth are preferably constructed as rounded-off nodules.

[0029] The profile is preferably constructed in such a way that the tissue is held by the profile in its tensioned position when the limbs are slightly opened. The profile acts therefore as an arrangement of barbs.

[0030] In a preferred embodiment the surface profile supporting the tensioning effect is constructed in such a way that at least one constriction is provided between the electrode parts. This is particularly efficient with electrode parts which have the same radii of curvature. This means that the

coagulation surfaces of the electrode parts, constructed in particular with the same radius of curvature, are preferably constructed at both end areas in such a way that while bringing the limbs together the tissue is transported in the direction of the end areas and is clamped in a respective constriction opposite the remaining area when the limbs have been brought together. This constriction has the additional advantage that the coagulation surfaces can essentially have a smooth construction and are thus easy to clean. Injury to the tissue is also avoided on account of the smooth surface.

[0031] In an advantageous embodiment an insulating section is formed on at least one of the coagulation surfaces, so that direct electrical contact between the coagulation surfaces can be prevented. Due to the heat conducting properties of the insulating section coagulation of the tissue is also guaranteed at this section. The insulating section depending on the construction of the electrode parts is to be provided at the areas of at least one coagulation surface which are closest to the opposite coagulation surface. This has to be taken into consideration in particular when the tensioning areas and thus the coagulation surfaces have a different radius of curvature. The insulating section is then preferably arranged at the central section of the tensioning area or tensioning areas, thus preventing a short circuit between the electrode parts. The tensioning effect is further enhanced simultaneously by the insulating section.

[0032] If the insulating section is constructed at the areas of at least one coagulation surface in closest proximity to the opposite coagulation surface it can close flush with the respective coagulation surface. The surface part of the coagulation surface which describes the area in closest proximity to the opposite coagulation surface must then be constructed from continuous insulating material, so that contact between the conductive areas of the coagulation surfaces is prevented. With convex or concave tensioning areas positioned opposite or coagulation surfaces having different radii of curvature the insulating section would have to be arranged along one crest of at least one coagulation surface. It is advantageous that the insulating section in this embodiment is protected by being housed in the respective electrode part and is thus safe from wear.

[0033] Alternatively, it is possible to construct the insulating surface in such a way that it protrudes from the respective coagulation surface. In this case the insulating section does not just serve the purpose of insulating, but also to bend the tissue to be treated several times in order to achieve better holding of the tissue between the distal ends of the electrosurgical instrument.

[0034] In a preferred embodiment the insulating section, that is to say the insulating section protruding from the respective coagulation surface, is constructed from several part sections. This facilitates an especially secure hold of the tissue between the electrode parts because the tissue is bent several times at the edges of the insulating section.

[0035] One solution according to the invention provides for constructing the insulating section itself to be structured in order to achieve an optimal hold of the tissue.

[0036] A preferred embodiment provides for the insulating section being constructed from ceramic or diamond. Advantageously both ceramic and diamond comprise amongst

other things a high corrosion resistance and high wear resistance to mechanical stress.

[0037] In a further preferred embodiment the insulating section is formed as the particular or each surface profile supporting the particular or each tensioning effect. A short circuit is thus prevented from occurring between the electrode parts in the simplest way as well as the tensioning of the tissue being increased.

[0038] A device preventing a short circuit between the electrode parts can, for example, also be provided at the limbs. If, for example, a spacer has been arranged thereon, the limbs cannot be brought together completely and a gap remains between the electrode parts.

[0039] Electrosurgical instruments of this kind can, for example, be constructed for use on an open body cavity. The principle of the electrode parts having a tensioning area can, however, also be employed for instruments used in endoscopies. The electrode parts attached to the limbs and if required the cutting instrument are then, for example, operated via a handle attached to a shaft or a control unit is provided, so that actuation of the electrode parts and/or the cutting instrument is controlled by the same. The electrosurgical instrument is thus preferably constructed as a laparoscopic instrument.

[0040] Further embodiments of the invention result from the sub claims.

[0041] In the following the invention is described from embodiment examples which are explained in more detail from the figures. These depict:

BRIEF DESCRIPTION OF THE DRAWINGS

[0042] FIG. 1 a schematic front view section of the electrode layout according to a first preferred embodiment;

[0043] FIG. 2 a perspective drawing of an electrosurgical instrument with an electrode layout according to the invention in a second preferred embodiment;

[0044] FIG. 3 the schematic front view section of the electrode layout according to the second preferred embodiment from FIG. 2;

[0045] FIG. 4 a schematic front view section of the electrode layout according to a third preferred embodiment;

[0046] FIG. 5 a schematic front view section of the electrode layout according to a fourth preferred embodiment.

DETAILED DESCRIPTION OF THE INVENTION

[0047] The same reference numerals will be used in the following description for the same parts and parts with the same function.

[0048] FIG. 1 shows a schematic front view section of the enlarged electrode layout according to a first preferred embodiment. The electrode layout is, for example, provided on an electrosurgical instrument, as described in more detail in FIG. 2. The electrode parts 22, 23 comprise open regions 22d, 23d which form a guide gap 24 for a cutting instrument 30. Due to the open regions 22d, 23d the electrode parts 22, 23 comprise two respective areas. The cutting instrument 30

can therefore be placed on the clamped tissue 40 for carrying out a cutting procedure. The guide gap 24 also facilitates a precise cut of the tissue 40, because the cutting instrument 30 can be guided along the guide gap 24. This is advantageous when the cutting instrument 30 is operated mechanically. As can be seen from the diagram the open regions 22d, 23d are aligned so as not to impede the cutting procedure. At least two areas of the respective electrode parts 22, 23 comprise respective separation surfaces 22e, 22e', 23e, 23e' opposite each other tapering in the direction of the coagulation surfaces 22a, 23a. The guide gap 24 thus expands in the direction facing away from a cutting area 25 between the electrode parts 22, 23 at each electrode part 22, 23.

[0049] Based on the tapered construction of the guide gap 24 precise guidance of the cutting instrument 30 is possible in the direct proximity of the cutting area 25 and a coagulation zone of the electrode parts 22, 23 is hardly disrupted. At the same time other areas of the guide gap 24 are easily accessible and thus also easy to clean. If the guide gap 24 has to be re-worked, for example, a coating has to be applied, this can then be carried out easily because of the improved access.

[0050] FIG. 2 shows a perspective drawing of an electrosurgical instrument with an electrode layout according to the invention in a second preferred embodiment. FIG. 3 shows the schematic front view section of the electrode layout according to the second preferred embodiment from FIG. 2. The instrument 10 is constructed for procedures on the open body cavity. Two limbs of the electrosurgical instrument 10 are identified in the figure by reference numbers 15 and 16. The two limbs 15, 16 are connected to each other via a spindle 17 and can swivel around the same. They comprise electrode parts 22, 23 fitted with distal ends 11, 12 wherein the electrode parts 22, 23 are positioned opposite each other. A vessel or tissue 40 can, for example, be gripped, and be coagulated by means of a HF current being passed through it, with the aid of the electrode parts 22, 23 which comprise coagulation surfaces 22a, 23a. Moreover, handles 18, 19 are provided which connect to the respective proximal ends 13, 14 of the limbs 15, 16. The proximal ends 13, 14 of the limbs 15, 16 each end in a current connection element or a current supply device 20, 21 for the connection of the electrosurgical instrument 10 to a HF generator (not depicted) which generates HF voltage, so that the HF current can, for example, be passed through the electric cables (not shown) running through the instrument 10 to the electrode parts 22, 23.

[0051] The electrode layout corresponds largely to that described in FIG. 1. The electrode parts 22, 23 comprise also in this embodiment two respective areas where respective separation surfaces 22e, 22e', 23e, 23e' positioned opposite each other tapering in the direction of the coagulation surface are provided. The guide gap 24 thus expands here also in the direction facing away from cutting area 25 between the electrode parts 22, 23 at each electrode part 22, 23. Due to the guide gap 24 the tissue 40 can be cut by means of a cutting instrument 30, while still being held by the electrode parts 22, 23.

[0052] The electrode parts 22, 23 are, however, constructed in such a way that one electrode part 23 covers the other electrode part 22 when the limbs 15, 16 are brought together. As can be seen from the figure the electrode parts

22, 23 comprise a curvature. One electrode part 22 has a convex curvature 22b and electrode part 23 positioned opposite the concave electrode part has a concave curvature 23b. The electrode parts 22 thus fit essentially positively together when the limbs 15, 16 are brought together. As a result of the curved electrode parts 22, 23 the tissue 40 is pulled in the direction of the end areas of electrode parts 22, 23, that is to say it is stretched in a direction of pull Z. The electrode parts 22, 23 thus form tensioning areas 22c, 23c. The tissue 40 is then easier to cut, as tissue fibres are aligned at right angles to a cutting direction and the tissue 40 becomes thinner in the procedure. Because of the tight fit the tissue 40 is fixed in a tensioned state between the limbs 15, 16. The electrode parts 22, 23 in this embodiment are essentially formed completely as tensioning areas 22c, 23c. Alternatively, it is possible that only sections of the electrode parts form tensioning areas.

[0053] The cutting instrument 30 comprises a blade 31 on a shaft and is housed during a coagulation phase within the limb 15. For the cutting procedure the cutting instrument 30 can be positioned on the already coagulated tissue and for cutting tissues 40 it can be moved at a defined feed rate. This occurs in this embodiment, for example, by means of a control unit (not shown) which controls the cutting instrument 30 and is activated by a finger switch 32. As the cutting instrument 30 is integrated in the electrosurgical instrument 10 a change of instruments and thus disruption of an operation procedure is avoidable.

[0054] Alternatively, it is possible for the user to actuate the cutting instrument 30 mechanically. The surgeon can then push the blade 31 when required through the limb 15 to and through the tissue. If no device for cutting the tissue is provided on the electrosurgical instrument the guide gap has then to be constructed in such a way that a cutting instrument being introduced from the outside, for example surgical scissors, can be placed with sufficient accuracy on the pretensioned tissue.

[0055] For a practical application a spacer (not shown) or similar device maintaining a gap between the electrode parts 22, 23 is constructed on the electrosurgical instrument 10, so that direct contact, and thus a short circuit, between the coagulation surfaces 22a, 23a of the electrode parts 22, 23 can be prevented. The spacer can, for example, be formed at one of the limbs 15, 16.

[0056] Alternatively, it is possible to construct the spacer as an insulating section on the electrode parts. Due to the heat conducting properties of the insulating section coagulation is also guaranteed at the same.

[0057] The electrosurgical instrument 10 shown in FIG. 2, as already mentioned, is constructed for use on the opened body cavity. The principle of the electrode parts having tapering separation surfaces can also be employed in endoscopy. The electrode parts attached to the limbs, and if required the cutting instrument, are then, for example, operated via a handle attached to a shaft or a control unit is provided so that actuation of the electrode parts and/or the cutting instrument is controlled by it.

[0058] FIGS. 4 and 5 respectively show an enlarged front view section of an electrode layout in a third and fourth embodiment. The electrode parts 22, 23 correspond essentially to the embodiment of that shown in FIGS. 2 and 3.

Moreover electrode parts **22**, **23** comprise also two respective areas, where separation surfaces **22e**, **22e'**, **23e**, **23e'** arranged opposite each other tapering in the direction of the coagulation surface **22a**, **23a** are provided. The guide gap **24** thus also expands here in the direction facing away from a cutting area **25** between the electrode parts **22**, **23** at each electrode part **22**, **23**.

[0059] In this embodiment the electrode part **22** has a convex curvature in a first central section while the electrode part **23** positioned opposite has a concave curvature in a second central section. A radius of curvature of the concave coagulation surface **23a** is greater than a radius of curvature of the convex coagulation surface **22a**. The curvatures **22b**, **23b** run along longitudinal axes of the distal ends **11**, **12** in such a way that a vessel or tissue **40** that is held between the distal ends **11**, **12** and extends perpendicularly to the longitudinal axes is held with a pressure that increases towards the first and second central sections. Due to the curvatures **22b**, **23b** the electrode parts **22**, **23** in these embodiments are also formed as tensioning areas **22c**, **23c**. As a result of the tensioning areas **22c**, **23c** the tissue **40** is stretched in a direction of pull **Z** towards the end regions of the electrode parts **22**, **23**. The fibres of the tissue **40** are thus aligned at right angles to a cutting direction, so that the tissue **40** is easier to cut.

[0060] FIG. 5 differs essentially from the electrode layout shown in FIG. 4 only in that a protruding insulating section **28**, formed from two part sections **28a**, **28a'**, is provided directly adjacent to an open region **22d** at the convex electrode part **22** which is divided by the open region **22d** into two areas. The part sections **28a**, **28a'** of the insulating section **28** extend preferably parallel to a crest of the electrode part **22**. Thus a short circuit between the electrode parts **22**, **23** is prevented when they are brought together. The part sections **28a**, **28a'** of the insulating section **28** support the tensioning effect of the tensioning area **22** on the one hand and facilitate bending of the clamped tissue **40** on the other. A reliable hold of the same between the electrode parts **22**, **23** is thus ensured.

[0061] Alternatively, it would be possible to construct the insulating section at the coagulation surface **22a** in such a way that it also extends continuously along the crest of the coagulation surface **22a**, but is essentially flush with it. The insulating section is then fitted into the coagulation surface **22a**. This is possible because the insulating section would be provided at the first central section of the coagulation surface **22a** and would thus reach the opposite coagulation surface **23a** first and exclusively when the limbs **15**, **16** are brought together. It would be advantageous if the insulating section in this embodiment is protected by being housed in the respective electrode part **22** and is thus safe from wear.

[0062] The insulating section **28** is preferably constructed from ceramic or diamond. Both materials show amongst other things a high corrosion resistance and high wear resistance to mechanical stress.

[0063] The electrode part **23** having a concave curvature **23b** comprises a saw tooth profile **27**, **27'** at the end areas. The teeth can, for example, be arranged in such a way that during the bringing together of the limbs they continue to grip the tissue **40** and transport it in the direction of pull **Z**. This increases the tension in the tissue **40** considerably. Care

must, however, be taken that injury to the tissue **40** caused by the profile is avoided, so the teeth are preferably constructed as nodules.

[0064] The nodules are preferably laid out in such a way that the tissue **40** is held by the profile **27**, **27'** in its tensioned position when the limbs are opened slightly. The profile **27**, **27'** acts therefore as an arrangement of barbs.

[0065] Alternatively or in addition it would be possible to construct the surface profile supporting the tensioning effect in such a way that in particular between the electrode parts having the same radius of curvature at least one constriction is provided. This means that the coagulation surfaces of the electrode parts are preferably constructed at both end areas in such a way that the tissue during the bringing together of the limbs is transported in the direction of the end areas and is clamped in a constriction opposite the remaining area when the limbs have been brought together. This constriction has the additional advantage that the coagulation surfaces can essentially have a smooth design and are thus easy to clean. Because of the smooth surface injury to the tissue is also avoided.

[0066] An insulating section arranged between the electrode surfaces can advantageously be constructed as a surface profile supporting a tensioning effect of the tensioning areas. A short circuit is thus prevented from occurring between the electrode parts in the simplest way as well as the tensioning of the tissue being increased.

[0067] At this juncture, it should be pointed out that all the parts described above have been claimed for themselves alone and in any combination, in particular the details represented in the drawings, as essential to the invention. Revisions to this are familiar to the man skilled in the art.

LIST OF REFERENCE NUMERALS

- [0068] **10** Electrosurgical instrument
- [0069] **11** Distal end
- [0070] **12** Distal end
- [0071] **13** Proximal end
- [0072] **14** Proximal end
- [0073] **15** Limb
- [0074] **16** Limb
- [0075] **17** Spindle
- [0076] **18** Handle
- [0077] **19** Handle
- [0078] **20** Current connection element, current supply device
- [0079] **21** Current connection element, current supply device
- [0080] **22** Electrode part
- [0081] **22a** Coagulation surface
- [0082] **22b** Convex curvature
- [0083] **22c** Tensioning area
- [0084] **22d** Open region

- [0085] 22e, 22e' Separation surface
- [0086] 23 Electrode part
- [0087] 23a Coagulation surface
- [0088] 23b Concave curvature
- [0089] 23c Tensioning area
- [0090] 23d Open region
- [0091] 23e, 23e' Separation surface
- [0092] 24 Guide gap
- [0093] 25 Cutting area
- [0094] 27, 27' Profile
- [0095] 28 Insulating section
- [0096] 28a, 28a' Part section of the insulating section
- [0097] 30 Cutting instrument
- [0098] 31 Blade
- [0099] 32 Finger switch
- [0100] 40 Tissue, vessel
- [0101] Z Direction of pull

1. Electrosurgical instrument including

two articulated limbs which can be actuated in the manner of a cutting or clamping tool,

electrode parts with coagulation surfaces positioned opposite each other at distal ends of the limbs for gripping tissue and adapted to pass a coagulating current through said tissue to cause its coagulation, at least one electrode part defining one open region adapted as a guide gap for a cutting instrument whereby said one electrode part is divided into at least two areas and said cutting instrument can be applied to clamped tissue for a cutting procedure, and

current supply devices for supplying the coagulation current to said electrode parts from a HF generator, and wherein

said at least two areas of said at least one electrode part define respective separation surfaces that are arranged opposite each other and that taper in the direction of said coagulation surfaces.

2. Electrosurgical instrument according to claim 1, wherein said opposite electrode parts both define said open regions that substantially align with one another which when said limbs are brought together.

3. Electrosurgical instrument according to claim 1 including a cutting instrument that is constructed as an integral part of the electrosurgical instrument.

4. Electrosurgical instrument according to claim 3, wherein said cutting instrument is adapted to be actuated by at least one of a mechanical or an electrical means.

5. Electrosurgical instrument according to claim 3, comprising a control unit and wherein said cutting instrument is

adapted for cutting by means of a HF current and is connected to said control unit, which controls supply of the cutting current depending on the operation phase.

6. Electrosurgical instrument according to claim 1, wherein the electrode parts each comprise at least one tensioning area adapted to tension tissue clamped between the electrode parts such that said tissue is pretensioned prior to a cutting procedure being carried out on the pretensioned tissue by the cutting instrument.

7. Electrosurgical instrument according to claim 6, wherein one of said tensioning areas defines a convex curvature in at least a first central section and an opposite said tensioning area comprises a concave curvature in at least a second central section such that when the limbs are brought together these tensioning areas fit together.

8. Electrosurgical instrument according to claim 6, wherein one of said tensioning areas defines at least a convex curvature in a first central section and an opposite said tensioning area defines a concave curvature in at least a second central section, the radius of curvature of the concave tensioning area being greater at least in the second central section than the radius of curvature of the convex tensioning area in the first central section and wherein said curvatures run along longitudinal axes of said distal ends in such a way that tissue clamped between the distal ends extends perpendicularly to said longitudinal axes and is retained by a pressure that increases in directions towards the first and second central sections.

9. Electrosurgical instrument according to claim 6, wherein at least one of a tensioning area and its opposing tensioning area defines a surface profile that produces the tensioning effect is constructed on the one tensioning areas and/or on the opposite tensioning area.

10. Electrosurgical instrument according to claim 9, wherein said surface profile is a saw tooth profile.

11. Electrosurgical instrument according to claim 9, wherein said surface profile is configured in such a way that at least one constriction is provided between the electrode parts.

12. Electrosurgical instrument according to claim 1, wherein an insulating section is provided on at least one coagulating surface that prevents direct electrical contact between the coagulating surfaces.

13. Electrosurgical instrument according to claim 12, wherein said insulating section comprises several segments.

14. Electrosurgical instrument according to claim 12, wherein said insulating section is structurally formed.

15. Electrosurgical instrument according to claim 12, wherein said insulating section is constructed from ceramic or from diamond.

16. Electrosurgical instrument according to claim 12, wherein said insulating section is configured as a surface profile that aids said tensioning effect.

17. Electrosurgical instrument according to claim 1 that is constructed as a laparoscopic instrument.

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专利名称(译)	电外科仪器		
公开(公告)号	US20080071268A1	公开(公告)日	2008-03-20
申请号	US11/573287	申请日	2005-07-15
[标]申请(专利权)人(译)	厄比电子医学有限责任公司		
申请(专利权)人(译)	ERBE ELEKTROMEDIZIN GMBH		
当前申请(专利权)人(译)	ERBE ELEKTROMEDIZIN GMBH		
[标]发明人	HAFNER DIETER		
发明人	HAFNER, DIETER		
IPC分类号	A61B18/14		
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优先权	102004039053 2004-08-11 DE 102004055669 2004-11-18 DE		
其他公开文献	US7799027		
外部链接	Espacenet USPTO		

摘要(译)

电外科器械技术领域本发明涉及一种电外科器械 (10) , 其包括两个臂 (15,16) , 所述两个臂具有铰接连接并且能够以切割或夹紧工具的方式致动。该器械还包括相对的电极部分 (22,23) , 在其肢体的远端 (11,12) 上具有凝固表面 (22a , 23a) , 用于保持血管或组织并使电流通过所述血管或组织凝固。后者, 其中至少一个电极部分具有开口区域 (22d , 23d) , 其用作切割器械 (30) 的引导间隙 (24) , 使得电极部分被分成至少两个可以将区域和切割器械放置在所保持的容器或组织上以执行切割操作。另外, 电流供应装置 (20,21) 将凝结电流从高频发生器提供给电极部分。所述电外科器械的改进构造允许电极部分上的开放区域提供切割器械的最佳引导, 由此所述开口区域可以容易地准备用于额外的切割操作和/或经受后处理。为实现此目的, 电极部分的两个或更多个开口区域包括朝向凝固表面逐渐变细的相应的相对的分表面 (22e , 22e' ; 23e , 23e') 。

