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(54) **SURGICAL STAPLING INSTRUMENT**

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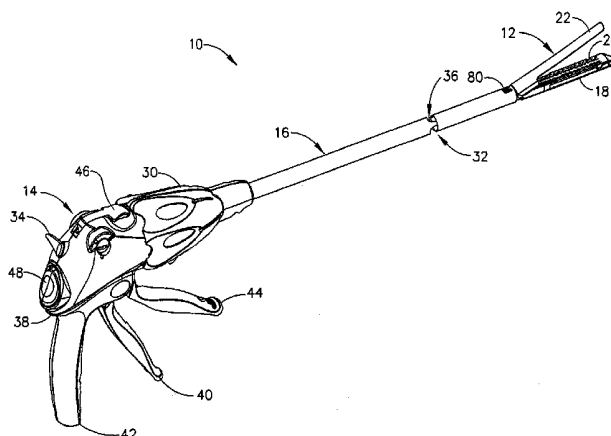
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(57) **ABSTRACT**

A surgical severing and stapling instrument, suitable for lap-
aroscopic and endoscopic clinical procedures, clamps tissue
within an end effector of an elongate channel pivotally
opposed by an anvil. An E-beam firing bar moves distally
through the clamped end effector to sever tissue and to drive
staples on each side of the cut. The E-beam firing bar affir-
matively spaces the anvil from the elongate channel to assure
properly formed closed staples, especially when an amount of
tissue is clamped that is inadequate to space the end effector.
In particular, an upper pin of the firing bar longitudinally
moves through an anvil slot and a channel slot is captured
between a lower cap and a middle pin of the firing bar to
assure a minimum spacing. Forming the E-beam from a thick-
ened distal portion and a thinned proximal strip enhances
manufacturability and facilitates use in such articulating sur-
gical instruments.

5 Claims, 13 Drawing Sheets



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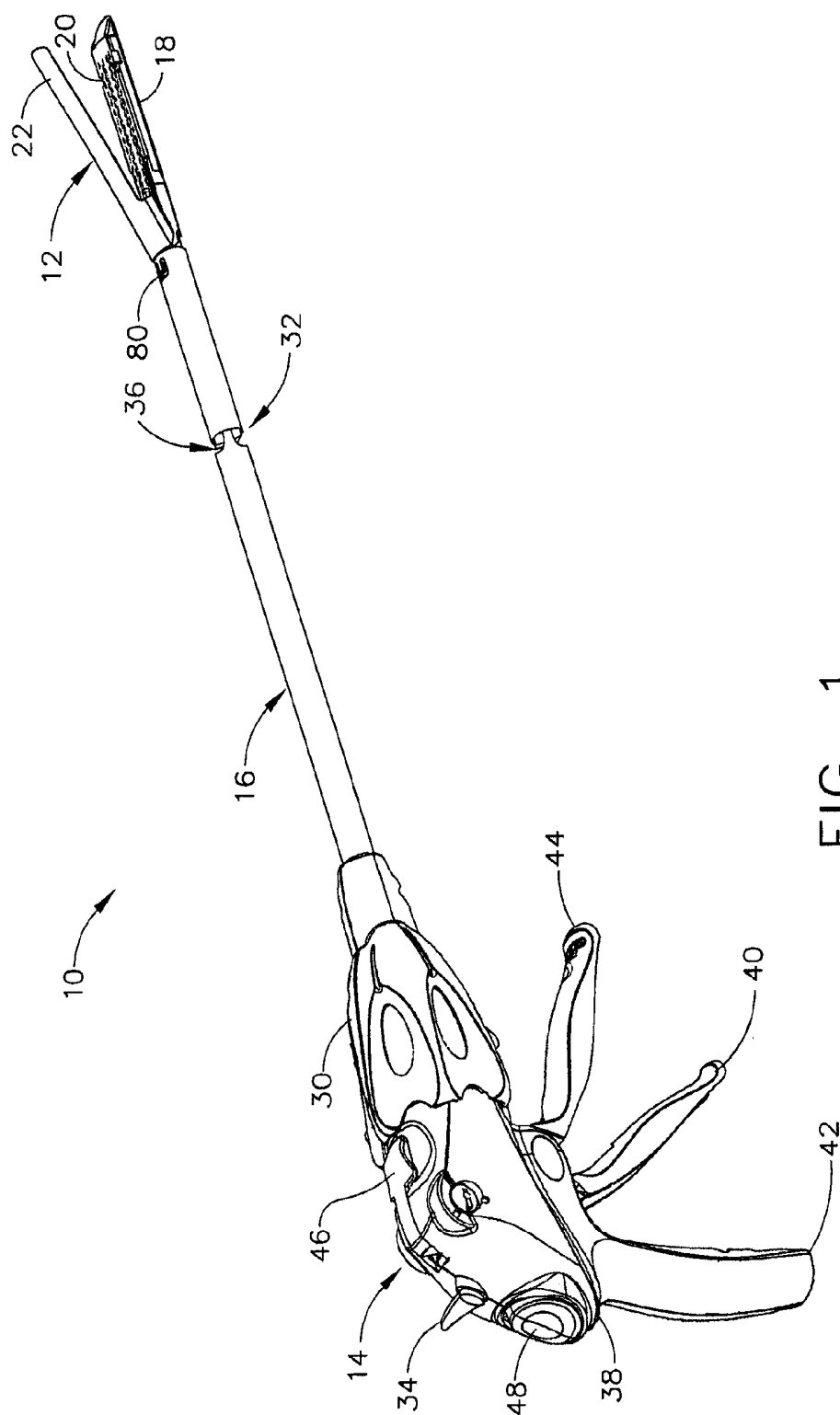


FIG. 1

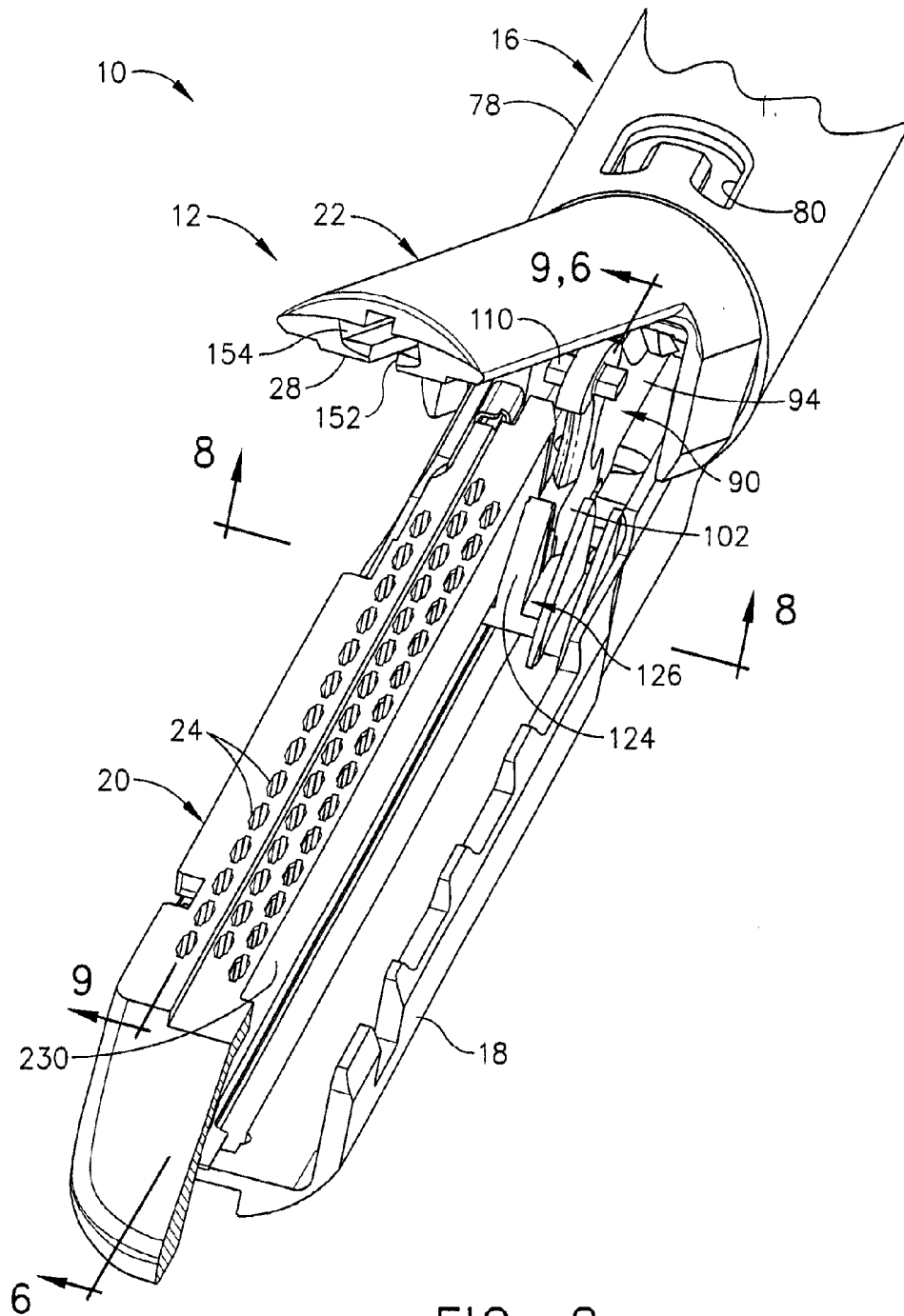


FIG. 2

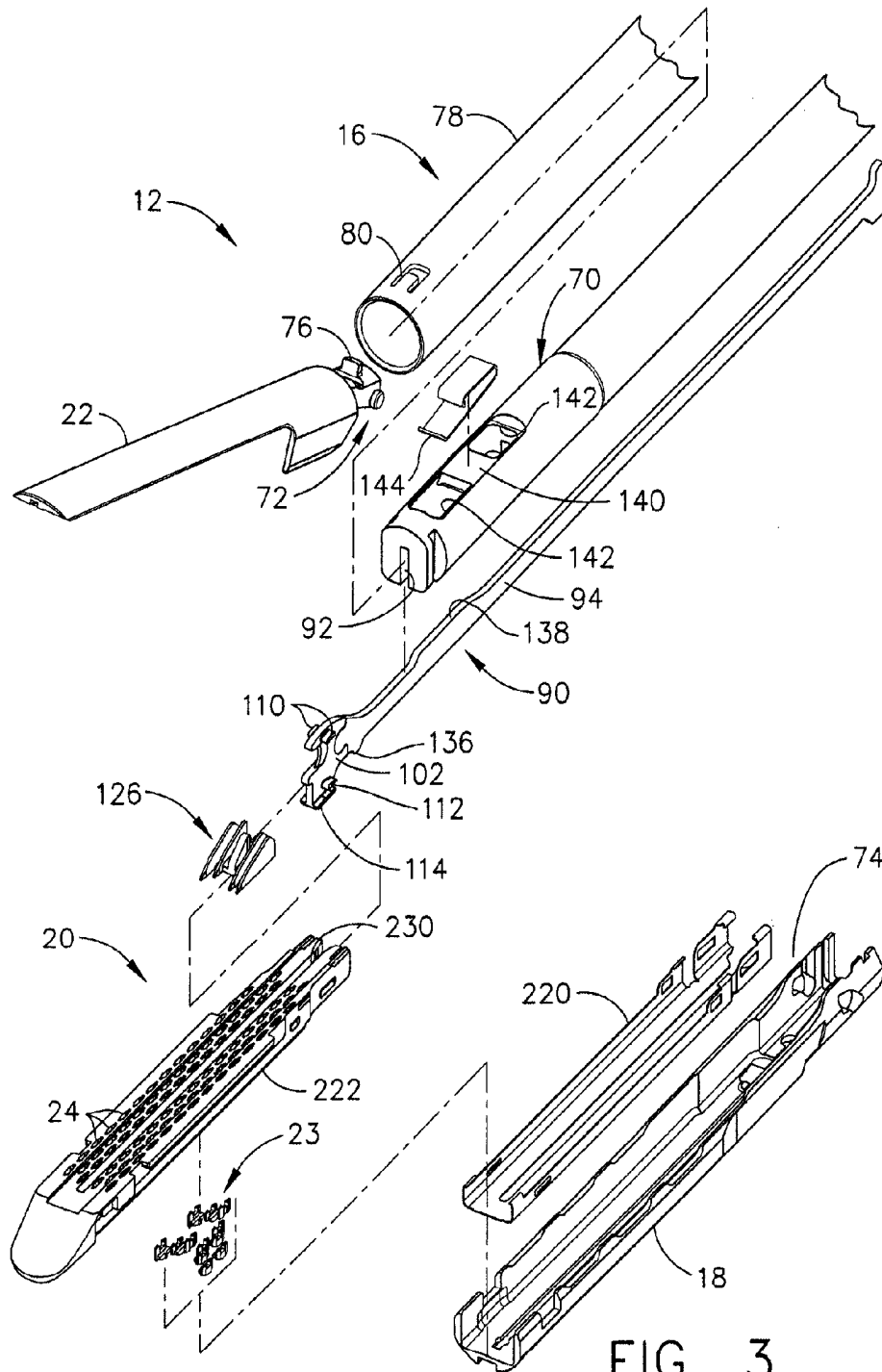


FIG. 3

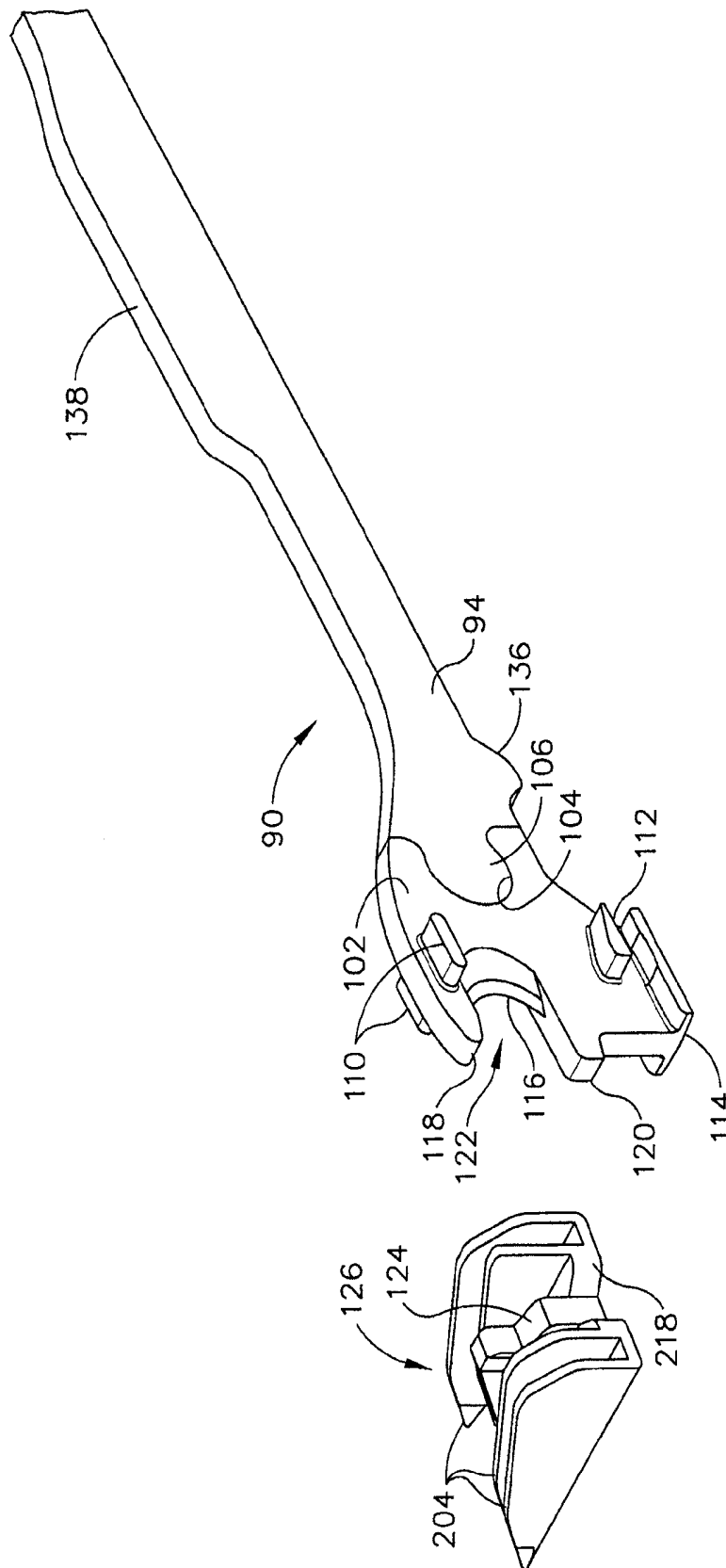


FIG. 4

FIG. 5

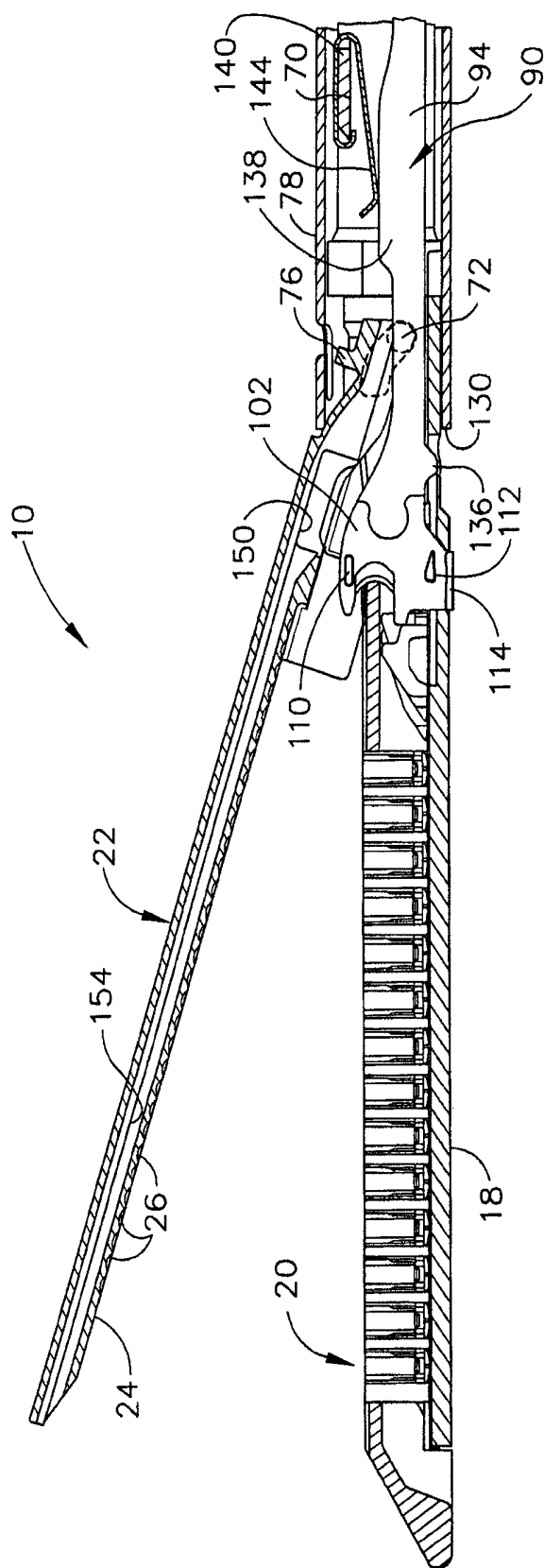


FIG. 6

FIG. 7

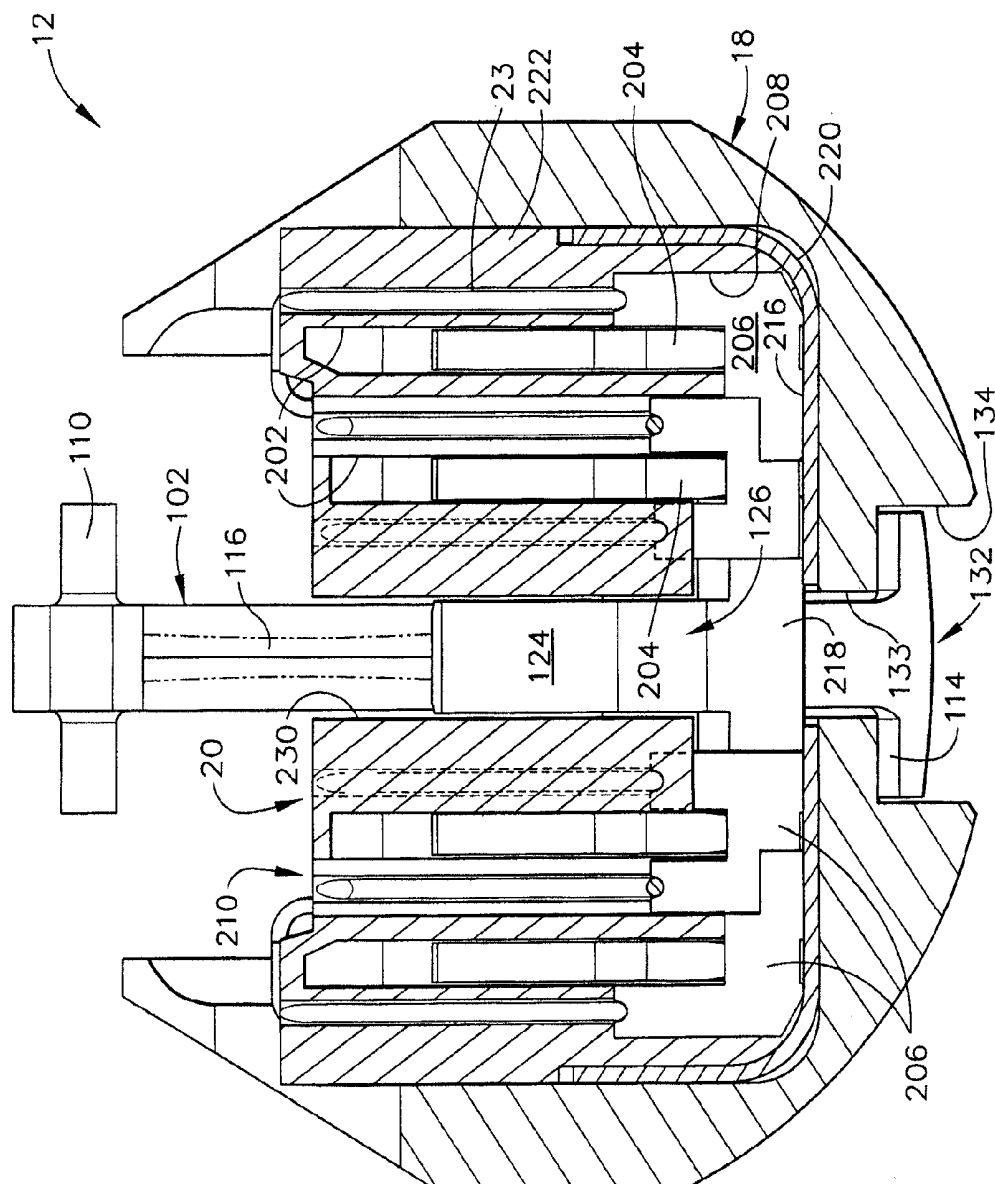


FIG. 8

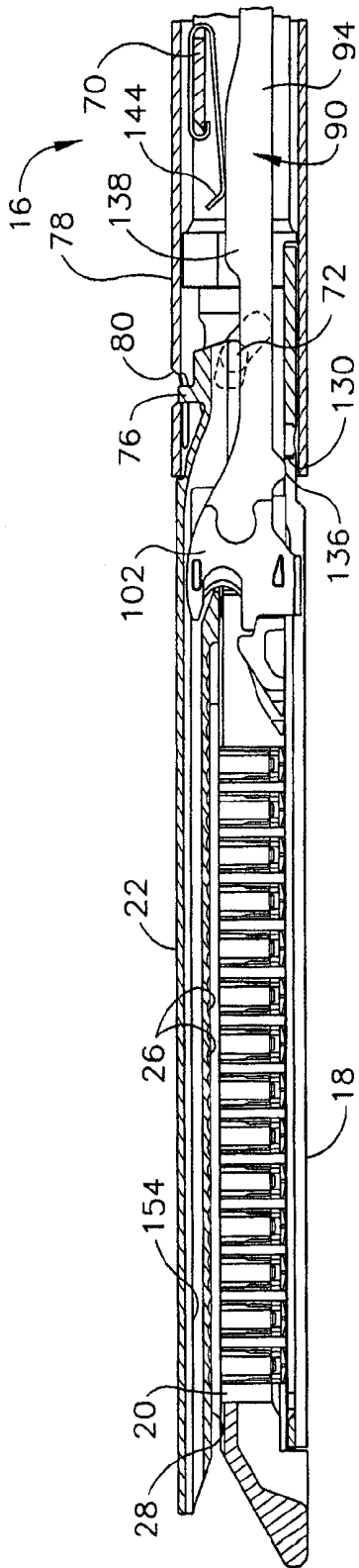


FIG. 9

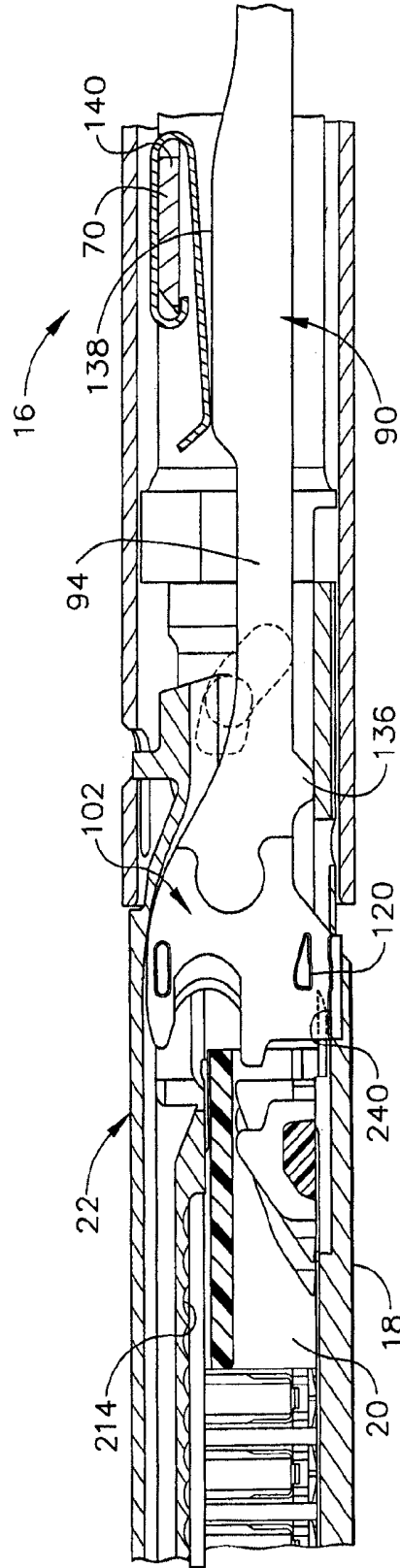


FIG. 10

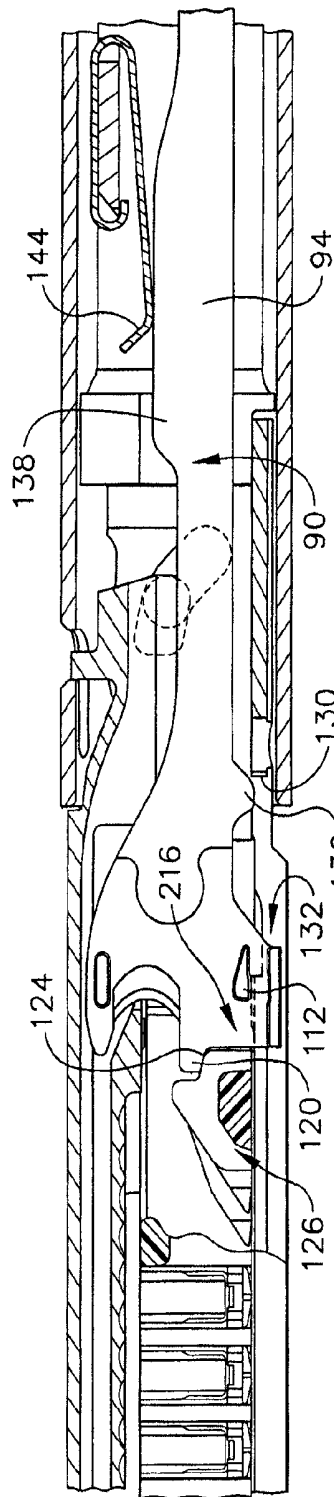


FIG. 11

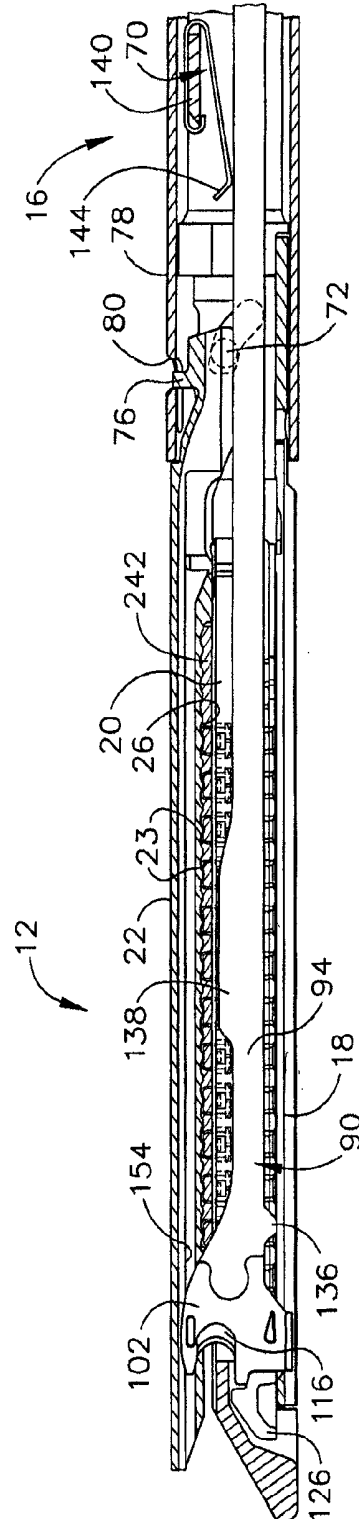
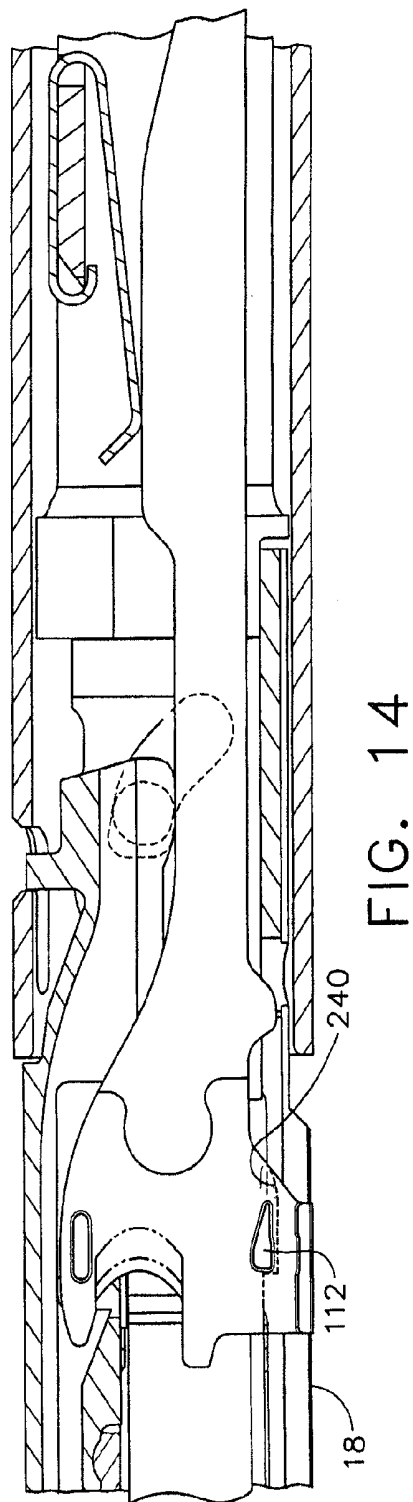
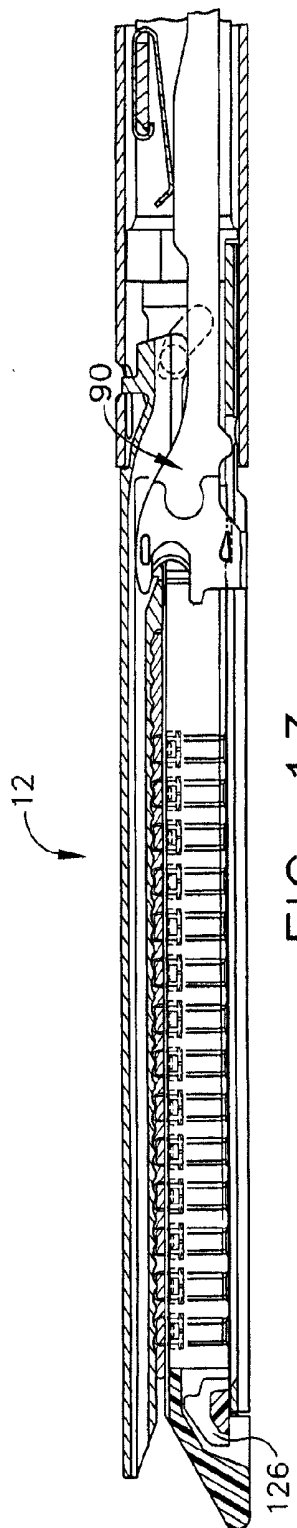


FIG. 12



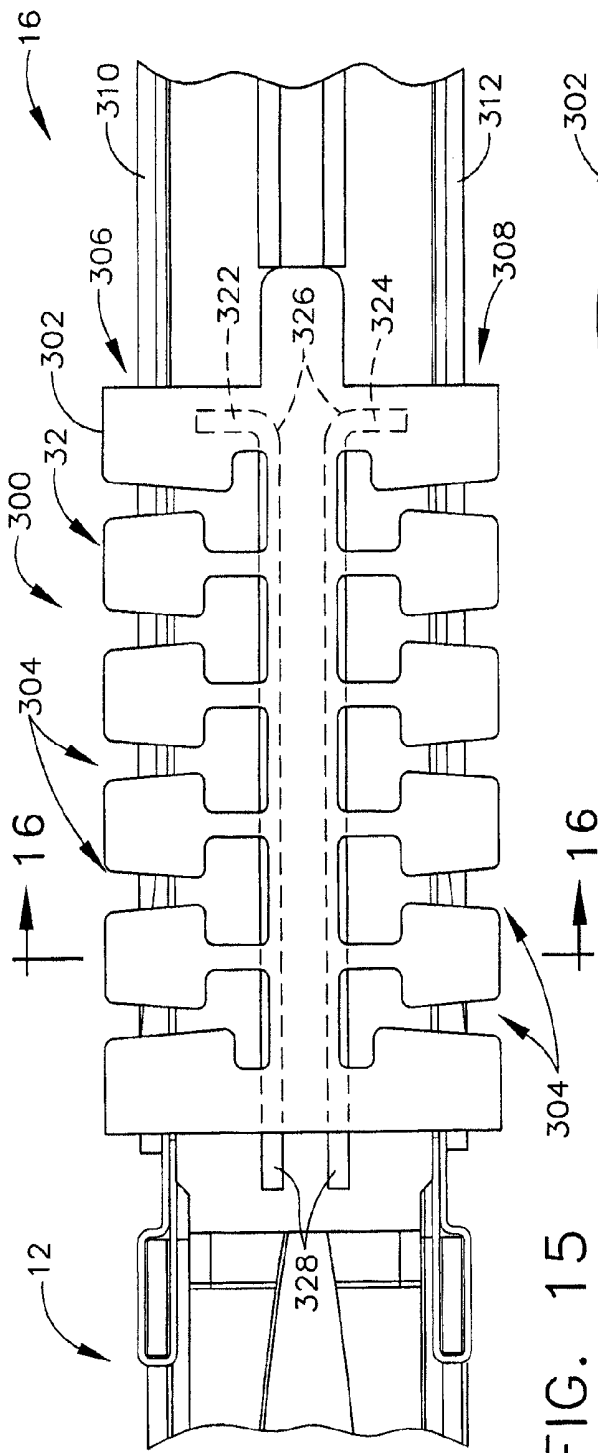


FIG. 15

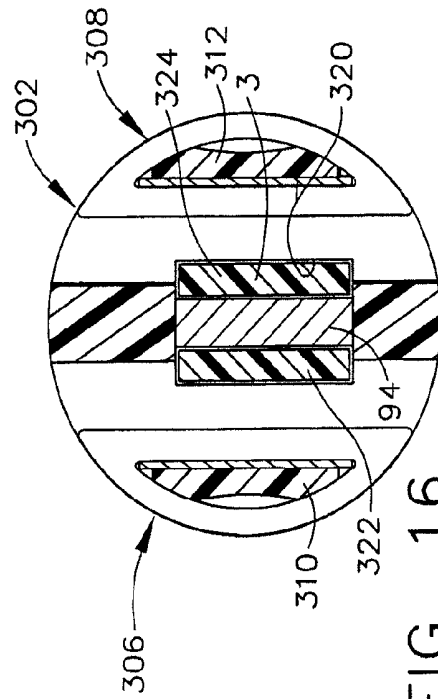


FIG. 16

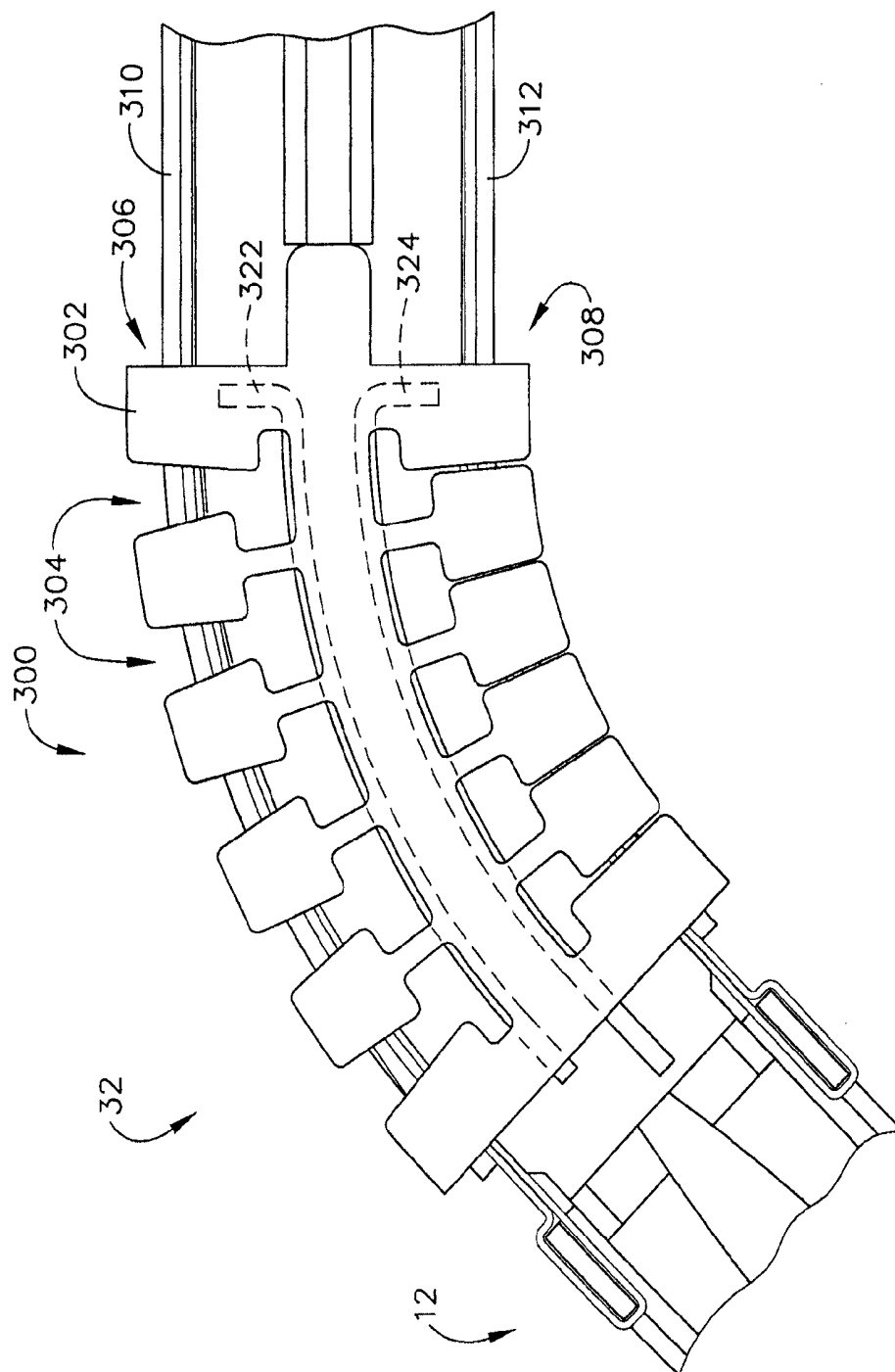
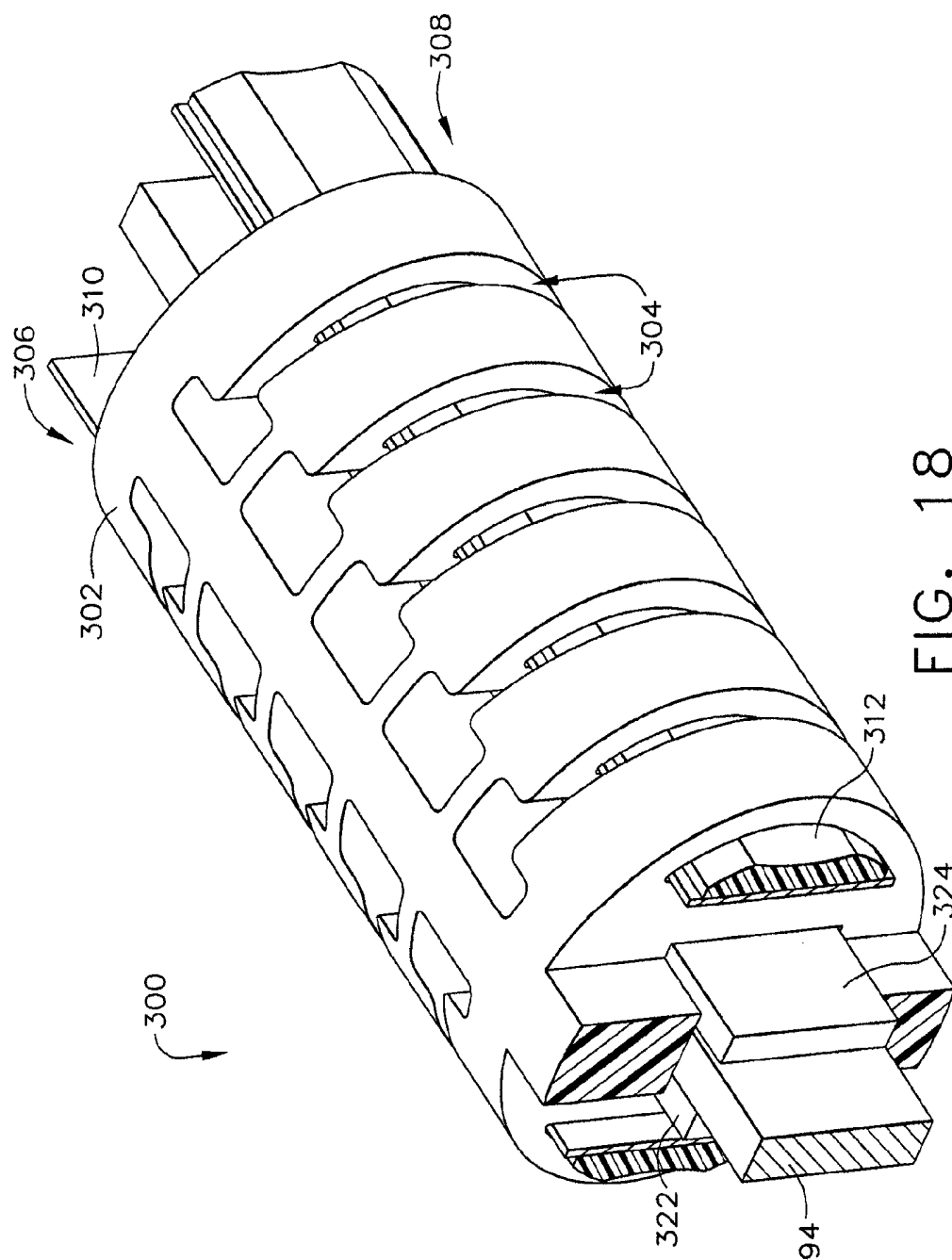


FIG. 17



SURGICAL STAPLING INSTRUMENT**CROSS-REFERENCE TO RELATED APPLICATIONS**

The present application is a continuation application under 35 U.S.C. § 120 of U.S. patent application Ser. No. 13/369,601, entitled ROBOTICALLY-CONTROLLED SURGICAL END EFFECTOR SYSTEM, filed on Feb. 9, 2012, now U.S. Pat. No. 8,783,541, which is a continuation application under 35 U.S.C. § 120 of U.S. patent application Ser. No. 13/118,246, entitled ROBOTICALLY-DRIVEN SURGICAL INSTRUMENT WITH E-BEAM DRIVER, filed on May 27, 2011, now U.S. Pat. No. 9,060,770, which is a continuation-in-part application under 35 U.S.C. § 120 of U.S. patent application Ser. No. 11/538,154, entitled ARTICULATING SURGICAL STAPLING INSTRUMENT INCORPORATING A TWO-PIECE E-BEAM FIRING MECHANISM, filed on Oct. 3, 2006, now U.S. Patent Application Publication No. 2007/0084897, the entire disclosures of which are incorporated by reference herein. The present application is a continuation application under 35 U.S.C. § 120 of U.S. patent application Ser. No. 11/141,753, entitled SURGICAL STAPLING INSTRUMENT HAVING AN ELECTROACTIVE POLYMER ACTUATED MEDICAL SUBSTANCE DISPENSER, filed on Jun. 1, 2005, now U.S. Pat. No. 8,905,977, which claims the benefit under 35 U.S.C. § 119(e) of U.S. Provisional Patent Application Ser. No. 60/591,694, entitled SURGICAL INSTRUMENT INCORPORATING AN ELECTRICALLY ACTUATED ARTICULATION MECHANISM, filed on Jul. 28, 2004, the entire disclosures of which are incorporated by reference herein.

FIELD OF THE INVENTION

The present invention relates in general to surgical instruments that are suitable for endoscopically inserting an end effector that is actuated by a longitudinally driven firing member, and more particularly a surgical stapling and severing instrument that has an articulating shaft.

BACKGROUND OF THE INVENTION

Endoscopic surgical instruments are often preferred over traditional open surgical devices since a smaller incision tends to reduce the post-operative recovery time and complications. Consequently, significant development has gone into a range of endoscopic surgical instruments that are suitable for precise placement of a distal end effector at a desired surgical site through a cannula of a trocar. These distal end effectors engage the tissue in a number of ways to achieve a diagnostic or therapeutic effect (e.g., endocutter, grasper, cutter, staplers, clip applier, access device, drug/gene therapy delivery device, and energy device using ultrasound, RF, laser, etc.).

Positioning the end effector is constrained by the trocar. Generally these endoscopic surgical instruments include a long shaft between the end effector and a handle portion manipulated by the clinician. This long shaft enables insertion to a desired depth and rotation about the longitudinal axis of the shaft, thereby positioning the end effector to a degree. With judicious placement of the trocar and use of graspers, for instance, through another trocar, often this amount of positioning is sufficient. Surgical stapling and severing instruments, such as described in U.S. Pat. No. 5,465,895, are an example of an endoscopic surgical instrument that successfully positions an end effector by insertion and rotation.

More recently, U.S. patent application Ser. No. 10/443,617, entitled SURGICAL STAPLING INSTRUMENT INCORPORATING AN E-BEAM FIRING MECHANISM, filed on May 20, 2003, now U.S. Pat. No. 6,978,921, which is incorporated by reference in its entirety, describes an improved "E-beam" firing bar for severing tissue and actuating staples. Some of the additional advantages include affirmatively spacing the jaws of the end effector, or more specifically a staple applying assembly, even if slightly too much or too little tissue is clamped for optimal staple formation. Moreover, the E-beam firing bar engages the end effector and staple cartridge in a way that enables several beneficial lock-outs to be incorporated.

Depending upon the nature of the operation, it may be desirable to further adjust the positioning of the end effector of an endoscopic surgical instrument. In particular, it is often desirable to orient the end effector at an axis transverse to the longitudinal axis of the shaft of the instrument. The transverse movement of the end effector relative to the instrument shaft is conventionally referred to as "articulation". This is typically accomplished by a pivot (or articulation) joint being placed in the extended shaft just proximal to the staple applying assembly. This allows the surgeon to articulate the staple applying assembly remotely to either side for better surgical placement of the staple lines and easier tissue manipulation and orientation. This articulated positioning permits the clinician to more easily engage tissue in some instances, such as behind an organ. In addition, articulated positioning advantageously allows an endoscope to be positioned behind the end effector without being blocked by the instrument shaft.

Approaches to articulating a surgical stapling and severing instrument tend to be complicated by integrating control of the articulation along with the control of closing the end effector to clamp tissue and fire the end effector (i.e., stapling and severing) within the small diameter constraints of an endoscopic instrument. Generally, the three control motions are all transferred through the shaft as longitudinal translations. For instance, U.S. Pat. No. 5,673,840 discloses an accordion-like articulation mechanism ("flex-neck") that is articulated by selectively drawing back one of two connecting rods through the implement shaft, each rod offset respectively on opposite sides of the shaft centerline. The connecting rods ratchet through a series of discrete positions.

Another example of longitudinal control of an articulation mechanism is U.S. Pat. No. 5,865,361 that includes an articulation link offset from a camming pivot such that pushing or pulling longitudinal translation of the articulation link effects articulation to a respective side. Similarly, U.S. Pat. No. 5,797,537 discloses a similar rod passing through the shaft to effect articulation.

In commonly owned U.S. patent application Ser. No. 10/615,973, entitled SURGICAL INSTRUMENT INCORPORATING AN ARTICULATION MECHANISM HAVING ROTATION ABOUT THE LONGITUDINAL AXIS, now U.S. Pat. No. 7,111,769, the disclosure of which is hereby incorporated by reference in its entirety, a rotational motion is used to transfer articulation motion as an alternative to a longitudinal motion.

In the application entitled SURGICAL STAPLING INSTRUMENT INCORPORATING AN E-BEAM FIRING MECHANISM, U.S. patent application Ser. No. 10/443,617, filed on May 20, 2003, now U.S. Pat. No. 6,978,921, the disclosure of which was previously incorporated by reference in its entirety, a surgical severing and stapling instrument, suitable for laparoscopic and endoscopic clinical procedures, clamps tissue within an end effector of an elongate channel pivotally opposed by an anvil. An E-beam firing bar moves

distally through the clamped end effector to sever tissue and to drive staples on each side of the cut. The E-beam firing bar affirmatively spaces the anvil from the elongate channel to assure properly formed closed staples, especially when an amount of tissue is clamped that is inadequate to space the end effector. In particular, an upper pin of the firing bar longitudinally moves through an anvil slot and a channel slot is captured between a lower cap and a middle pin of the firing bar to assure a minimum spacing. While this E-beam firing bar has a number of advantages, additional features are desirable to enhance manufacturability and to minimize dimensional variations.

Consequently, a significant need exists for a surgical instrument with a firing bar that advantageously assures proper spacing between clamped jaws of an end effector and which facilitates articulation of its shaft.

BRIEF DESCRIPTION OF THE FIGURES

The accompanying drawings, which are incorporated in and constitute a part of this specification, illustrate embodiments of the invention, and, together with the general description of the invention given above, and the detailed description of the embodiments given below, serve to explain the principles of the present invention.

FIG. 1 is a perspective view of an endoscopic surgical stapling instrument for surgical stapling and severing in an open, unarticulated state.

FIG. 2 is a left, front perspective view of an open staple applying assembly of the surgical stapling instrument of FIG. 1 with a right half portion of a replaceable staple cartridge included in a staple channel.

FIG. 3 is an exploded perspective view of the staple applying assembly of FIG. 2 with a complete replaceable staple cartridge and an alternative nonarticulating shaft configuration.

FIG. 4 is a perspective view of a two-piece knife and firing bar ("E-beam") of the staple applying assembly of FIG. 2.

FIG. 5 is a perspective view of a wedge sled of a staple cartridge of the staple applying assembly of FIG. 1.

FIG. 6 is a left side view in elevation taken in longitudinal cross section along a centerline line 6-6 of the staple applying assembly of FIG. 2.

FIG. 7 is a perspective view of the open staple applying assembly of FIG. 2 without the replaceable staple cartridge, a portion of the staple channel proximate to a middle pin of two-piece knife and firing bar, and without a distal portion of a staple channel.

FIG. 8 is a front view in elevation taken in cross section along line 8-8 of the staple applying assembly of FIG. 2 depicting internal staple drivers of the staple cartridge and portions of the two-piece knife and firing bar.

FIG. 9 is a left side view in elevation taken generally along the longitudinal axis of line 6-6 of a closed staple applying assembly of FIG. 2 to include center contact points between the two-piece knife and wedge sled but also laterally offset to show staples and staple drivers within the staple cartridge.

FIG. 10 is a left side detail view in elevation of the staple applying assembly of FIG. 9 with the two-piece knife retracted slightly more as typical for staple cartridge replacement.

FIG. 11 is a left side detail view in elevation of the staple applying assembly of FIG. 10 with the two-piece knife beginning to fire, corresponding to the configuration depicted in FIG. 9.

FIG. 12 is a left side cross-sectional view in elevation of the closed staple applying assembly of FIG. 9 after the two-piece knife and firing bar has distally fired.

FIG. 13 is a left side cross-sectional view in elevation of the closed staple applying assembly of FIG. 12 after firing of the staple cartridge and retraction of the two-piece knife.

FIG. 14 is a left side cross-sectional detail view in elevation of the staple applying assembly of FIG. 13 with the two-piece knife allowed to drop into a lockout position.

FIG. 15 is a top view in section taken along lines 15-15 of an articulation joint (flex neck) of the surgical stapling instrument of FIG. 1.

FIG. 16 is a front view in elevation taken in vertical cross section along lines 16-16 of the articulation joint of FIG. 15, showing electroactive polymer (EAP) plate articulation actuators and EAP support plates for a firing bar.

FIG. 17 is a top view in section along lines 15-15 of the articulation joint of FIG. 16 after articulation.

FIG. 18 is a perspective view of the articulation joint of FIG. 15.

DETAILED DESCRIPTION OF THE INVENTION

The entire disclosure of U.S. patent application Ser. No. 11/082,495, entitled SURGICAL INSTRUMENT INCORPORATING AN ELECTRICALLY ACTUATED ARTICULATION MECHANISM, filed on Mar. 17, 2005, now U.S. Pat. No. 7,506,790, is incorporated herein by reference. The entire disclosure of U.S. Pat. No. 6,667,825, entitled STABLE CONJUGATED POLYMER ELECTROCHROMIC DEVICES INCORPORATING IONIC LIQUIDS, issued on Jan. 3, 2002, is incorporated herein by reference. The entire disclosure of U.S. patent application Ser. No. 11/061,908, entitled SURGICAL INSTRUMENT INCORPORATING A FLUID TRANSFER CONTROLLED ARTICULATION MECHANISM, filed on Feb. 18, 2005, now U.S. Pat. No. 7,559,450, is incorporated herein by reference.

In FIGS. 1-3, a surgical stapling instrument 10 has at its distal end an end effector, depicted as a staple applying assembly 12, spaced apart from a handle 14 (FIG. 2) by an elongate shaft 16. The staple applying assembly 12 includes a staple channel 18 for receiving a replaceable staple cartridge 20. Pivotaly attached to the staple channel 18 is an anvil 22 that clamps tissue to the staple cartridge 20 and serves to deform staples 23 (FIG. 3) driven up from staple holes 24 in the staple cartridge 20 against staple forming recesses 26 (FIG. 6) in an anvil undersurface 28 into a closed shape. When the staple applying assembly 12 is closed, its cross sectional area, as well as the elongate shaft 16 are suitable for insertion through a small surgical opening, such as through a cannula of a trocar (not shown).

With particular reference to FIG. 1, correct placement and orientation of the staple applying assembly 12 is facilitated by controls on the handle 14. In particular, a rotation knob 30 causes rotation of the shaft 16 about its longitudinal axis, and hence rotation of the staple applying assembly 12. Additional positioning is enabled at an articulation joint 32 in the shaft 16 that pivots the staple applying assembly 12 in an arc from the longitudinal axis of the shaft 16, thereby allowing placement behind an organ or allowing other instruments such as an endoscope (not shown) to be oriented behind the staple applying assembly 12. This articulation is advantageously effected by an articulation control switch 34 on the handle 14 that transmits an electrical signal to the articulation joint 32 to an

Electroactive Polymer (EAP) actuator **36**, powered by an EAP controller and power supply **38** contained within the handle **14**.

Once positioned with tissue in the staple applying assembly **12**, a surgeon closes the anvil **22** by drawing a closure trigger **40** proximally toward a pistol grip **42**. Once clamped thus, the surgeon may grasp a more distally presented firing trigger **44**, drawing it back to effect firing of the staple applying assembly **12**, which in some applications is achieved in one single firing stroke and in other applications by multiple firing strokes. Firing accomplishes simultaneously stapling of at least two rows of staples while severing the tissue therebetween.

Retraction of the firing components may be automatically initiated upon full travel. Alternatively, a retraction lever **46** may be drawn aft to effect retraction. With the firing components retracted, the staple applying assembly **12** may be unclamped and opened by the surgeon slightly drawing the closure trigger **40** aft toward the pistol grip **42** and depressing a closure release button **48** and then releasing the closure trigger **40**, thereby releasing the two stapled ends of severed tissue from the staple applying assembly **12**.

Staple Applying Assembly

While an articulation joint **32** is depicted in FIG. **1**, for clarity and as an alternative application, the surgical stapling instrument **10** of FIGS. **2-14** omit an articulation joint **32**. It should be appreciated, however, that aspects of the present invention have particular advantages for articulation as described below with regard to FIGS. **15-18**.

In FIGS. **1-3**, the staple applying assembly **12** accomplishes the functions of clamping onto tissue, driving staples and severing tissue by two distinct motions transferred longitudinally down the shaft **16** over a shaft frame **70**. This shaft frame **70** is proximally attached to the handle **14** and coupled for rotation with the rotation knob **30**. An illustrative multi-stroke handle **14** for the surgical stapling and severing instrument **10** of FIG. **1** is described in greater detail in the co-owned U.S. patent application Ser. No. 10/674,026, entitled SURGICAL STAPLING INSTRUMENT INCORPORATING A MULTISTROKE FIRING POSITION INDICATOR AND RETRACTION MECHANISM, now U.S. Pat. No. 7,364,061, the disclosure of which is hereby incorporated by reference in its entirety, with additional features and variation as described herein. While a multi-stroke handle **14** advantageously supports applications with high firing forces over a long distance, applications consistent with the present invention may incorporate a single firing stroke, such as described in commonly owned U.S. patent application Ser. No. 10/441,632, entitled SURGICAL STAPLING INSTRUMENT HAVING SEPARATE DISTINCT CLOSING AND FIRING SYSTEMS, now U.S. Pat. No. 7,000,818, the disclosure of which is hereby incorporated by reference in its entirety.

With particular reference to FIG. **3**, the distal end of the shaft frame **70** is attached to the staple channel **18**. The anvil **22** has a proximal pivoting end **72** that is pivotally received within a proximal end **74** of the staple channel **18**, just distal to its engagement to the shaft frame **70**. The pivoting end **72** of the anvil **22** includes a closure feature **76** proximate but distal to its pivotal attachment with the staple channel **18**. Thus, a closure tube **78**, whose distal end includes a horseshoe aperture **80** that engages this closure feature **76**, selectively imparts an opening motion to the anvil **22** during proximal longitudinal motion and a closing motion to the anvil **22** during distal longitudinal motion of the closure tube **78** sliding over the shaft frame **70** in response to the closure trigger **40**.

The shaft frame **70** encompasses and guides a firing motion from the handle **14** through a longitudinally reciprocating, two-piece knife and firing bar **90**. In particular, the shaft frame **70** includes a longitudinal firing bar slot **92** that receives a proximal portion of the two-piece knife and firing bar **90**, specifically a laminate tapered firing bar **94**. It should be appreciated that the laminated tapered firing bar **94** may be substituted with a solid firing bar or of other materials in applications not intended to pass through an articulation joint, such as depicted in FIGS. **2-14**.

An E-beam **102** is the distal portion of the two-piece knife and firing bar **90**, which facilitates separate closure and firing as well as spacing of the anvil **22** from the elongate staple channel **18** during firing. With particular reference to FIGS. **3-4**, in addition to any attachment treatment such as brazing or an adhesive, the knife and firing bar **90** are formed of a female vertical attachment aperture **104** proximally formed in the E-beam **102** that receives a corresponding male attachment member **106** distally presented by the laminated tapered firing bar **94**, allowing each portion to be formed of a selected material and process suitable for their disparate functions (e.g., strength, flexibility, friction). The E-beam **102** may be advantageously formed of a material having suitable material properties for forming a pair of top pins **110**, a pair of middle pins **112** and a bottom pin or foot **114**, as well as being able to acquire a sharp cutting edge **116**. In addition, integrally formed and proximally projecting top guide **118** and middle guide **120** bracketing each vertical end of the cutting edge **116** further define a tissue staging area **122** assisting in guiding tissue to the sharp cutting edge **116** prior to being severed. The middle guide **120** also serves to engage and fire the staple applying apparatus **12** by abutting a stepped central member **124** of a wedge sled **126** (FIG. **5**) that effects staple formation by the staple applying assembly **12**, as described in greater detail below.

Forming these features (e.g., top pins **110**, middle pins **112**, and bottom foot **114**) integrally with the E-beam **102** facilitates manufacturing at tighter tolerances relative to one another as compared to being assembled from a plurality of parts, ensuring desired operation during firing and/or effective interaction with various lockout features of the staple applying assembly **12**.

In FIGS. **6-7**, the surgical stapling instrument **10** is shown open, with the E-beam **102** fully retracted. During assembly, the lower foot **114** of the E-beam **102** is dropped through a widened hole **130** in the staple channel **18** and the E-beam **102** is then advanced such that the E-beam **102** slides distally along a lower track **132** formed in the staple channel **18**. In particular, the lower track **132** includes a narrow slot **133** that opens up as a widened slot **134** on an undersurface of the staple channel **18** to form an inverted T-shape in lateral cross section, as depicted particularly in FIGS. **7** and **8**, which communicates with the widened hole **130**. Once assembled, the components proximally coupled to the laminate tapered firing bar **94** do not allow the lower foot **114** to proximally travel again to the widened hole **130** to permit disengagement.

In FIG. **9**, the laminate tapered firing bar **94** facilitates insertion of the staple applying assembly **12** through a trocar. In particular, a more distal, downward projection **136** raises the E-beam **102** when fully retracted. This is accomplished by placement of the downward projection **136** at a point where it cams upwardly on a proximal edge of the widened hole **130** in the staple channel **18**.

In FIG. **10**, the laminate tapered firing bar **94** also enhances operation of certain lockout features that may be incorporated into the staple channel **18** by including a more proximal upward projection **138** that is urged downwardly by the shaft

frame 70 during an initial portion of the firing travel. In particular, a lateral bar 140 is defined between a pair of square apertures 142 in the shaft frame 70 (FIG. 3). A clip spring 144 that encompasses the lateral bar 140 downwardly urges a portion of the laminate tapered firing bar 94 projecting distally out of the longitudinal firing bar slot 92, which ensures certain advantageous lockout features are engaged when appropriate. This urging is more pronounced or confined solely to that portion of the firing travel when the upward projection 138 contacts the clip spring 144.

In FIGS. 6-7, the E-beam 102 is retracted with the top pins 110 thereof residing within an anvil pocket 150 near the pivoting proximal end of the anvil 22. A downwardly open vertical anvil slot 152 (FIG. 2) laterally widens in the anvil 22 into an anvil internal track 154 that captures the top pins 110 of the E-beam 102 as they distally advance during firing, as depicted in FIGS. 9-10, affirmatively spacing the anvil 22 from the staple channel 18. Thus, with the E-beam 102 retracted, the surgeon is able to repeatedly open and close the staple applying assembly 12 until satisfied with the placement and orientation of tissue captured therein for stapling and severing, yet the E-beam 102 assists in proper positioning of tissue even for a staple applying assembly 12 of reduced diameter and correspondingly reduced rigidity.

In FIGS. 2-3, 5-6, 8-14, the staple applying assembly 12 is shown with the replaceable staple cartridge 20 that includes the wedge sled 126. Longitudinally aligned and parallel plurality of downwardly open wedge slots 202 (FIG. 8) receive respective wedges 204 integral to the wedge sled 126. In FIGS. 8-10, the wedge sled 126 thus cams upwardly a plurality of staple drivers 206 that are vertically slidable within staple driver recesses 208. In this illustrative version, each staple driver 206 includes two vertical prongs, each translating upwardly into a respective staple hole 210 to upwardly force out and deform a staple 23 resting thereupon against a staple forming surface 214 (FIG. 10) of the anvil 22. A central firing recess 216 (FIG. 3) defined within the staple cartridge 20 proximate to the staple channel 18 allows the passage of the bottom, horizontal portion 218 (FIG. 5) of the wedge sled 126 as well as the middle pins 112 of the E-beam 102. Specifically, a staple cartridge tray 220 (FIGS. 3, 8) attaches to and underlies a polymer staple cartridge body 222 that has the staple driver recesses 208, staple holes 210, and central firing recess 216 formed therein. As staples 23 are thus formed to either side, the sharp cutting edge 116 enters a vertical through slot 230 passing through the longitudinal axis of the staple cartridge 20, excepting only a most distal end thereof.

Firing the staple applying assembly 12 begins as depicted in FIG. 10 with the two-piece knife and firing bar 90 proximally drawn until the downward projection 136 cams the middle guide 120 on the E-beam 102 upward and aft, allowing a new staple cartridge 20 to be inserted into the staple channel 18 when the anvil 22 is open as depicted in FIGS. 2, 6.

In FIG. 11, the two-piece knife and firing bar 90 has been distally advanced a small distance, allowing the downward projection 136 to drop into the widened hole 130 of the lower track 132 under the urging of the clip spring 144 against the upward projection 138 of the laminate tapered firing bar 94. The middle guide 120 prevents further downward rotation by resting upon the stepped central member 124 of the wedge sled 126, thus maintaining the middle pin 112 of the E-beam within the central firing recess 216.

In FIG. 12, the two-piece knife and firing bar 90 has been distally fired, advancing the wedge sled 126 to cause formation of staples 23 while severing tissue 242 clamped between the anvil 22 and staple cartridge 20 with the sharp cutting edge

116. Thereafter, in FIG. 13, the two-piece knife and firing bar 90 is retracted, leaving the wedge sled 126 distally positioned.

In FIG. 14, the middle pin 112 is allowed to translate down into a lockout recess 240 formed in the staple channel 18 (also see FIGS. 7, 10). Thus, the operator would receive a tactile indication as the middle pin 112 encounters the distal edge of the lockout recess 240 when the wedge sled 126 (not shown in FIG. 14) is not proximally positioned (i.e., missing staple cartridge 20 or spent staple cartridge 20).

In FIG. 1, an articulation joint 32 is depicted that advantageously benefits from the flexible strength of the two-piece knife and firing bar 90. In FIGS. 15-18, the articulation joint 32 is depicted as a flex neck joint 300 formed by vertebral column body 302 having laterally symmetric pairs of arcing recesses 304 that allow articulation in an articulation plane. It is generally known to simultaneously compress and expand respective lateral sides 306, 308 by selective movement of control rods (not shown) that longitudinally pass through the respective lateral sides 306, 308. Depicted, however, are EAP plate actuators 310, 312, each capable of powered deflection to one or both lateral directions.

A central passage 320 (FIG. 16) defined longitudinally through the vertebral column body 302 receives a pair of support plates 322, 324 that prevent buckling and binding of the laminate tapered firing bar 94. In the illustrative version, each support plate 322, 324 has a proximal fixed end 326 (FIG. 15) and a sliding end 328 to accommodate changes in radial distance during articulation. Having a firing bar 94 of a thinner thickness is thus supported.

While the present invention has been illustrated by description of several embodiments and while the illustrative embodiments have been described in considerable detail, it is not the intention of the applicant to restrict or in any way limit the scope of the appended claims to such detail. Additional advantages and modifications may readily appear to those skilled in the art.

For example, while there are a number of advantages to having a wedge sled integral to a staple cartridge, in some applications consistent with aspects of the present invention, the wedge sled may be integral instead to an E-beam. For instance, an entire end effector may be replaceable rather than just the staple cartridge.

What is claimed is:

1. A surgical instrument, comprising:

a handle, comprising:

a closure system configured to generate a closing motion when actuated;

a closure release system configured to releasably hold said closure system in an actuated condition; and

a firing system configured to generate a distal firing motion and a proximal return motion;

a shaft extending from said handle;

an articulation joint, wherein said firing system is configured to traverse said articulation joint;

an end effector movable relative to said shaft about said articulation joint, wherein said end effector comprises:

a first jaw member; and

a second jaw member; and

a longitudinally extending member, wherein said longitudinally extending member is configured to be moved between a proximal position and a distal position, and wherein said longitudinally extending member is configured to contact one of said first jaw member and said second jaw member in response to said distal firing motion and control the position of said first jaw member relative to said second jaw member as said longitudinally

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nally extending member is pushed distally from said proximal position to said distal position.

2. The surgical instrument of claim 1, further comprising a staple cartridge including a plurality of staples removably stored therein.

3. A surgical instrument, comprising:

a handle;

a closure system configured to generate a closing motion when actuated, wherein said closure system comprises an open condition and a closed condition;

a firing system configured to generate a firing motion and a return motion, wherein said closure system is held in said closed condition when said firing system is generating said firing motion, and wherein said firing system comprises a longitudinal member;

a shaft extending from said handle, wherein said shaft comprises:

a closure member configured to transmit said closing motion; and

a firing member configured to transmit said firing motion;

an articulation joint, wherein said firing system is configured to traverse said articulation joint during said firing motion and said return motion; and

an end effector including a first jaw and a second jaw, wherein said first jaw is movable relative to said second jaw, wherein said first jaw is responsive to said closing motion,

wherein said end effector is movable relative to said shaft about said articulation joint, and wherein said longitudinal member is configured to contact one of said first jaw member and said second jaw member in response to said firing motion and control the position of said first jaw member relative to said second jaw member as said longitudinal member is pushed distally during said firing motion.

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4. The surgical instrument of claim 3, further comprising a staple cartridge including a plurality of staples removably stored therein.

5. A surgical instrument, comprising:

a handle;

a closure system configured to generate a closing motion when actuated;

a firing system configured to generate a firing motion when actuated;

a shaft extending from said handle;

a lock system;

an articulation joint;

an end effector movable relative to said shaft about said articulation joint, wherein said end effector comprises:

a staple cartridge including a plurality of staples removably stored therein;

a sled, wherein said sled is configured to be distally pushed by said firing system;

a first jaw; and

a second jaw, wherein said first jaw is rotatable relative to said second jaw;

a closure member responsive to said closing motion, wherein said closure member is configured to engage said first jaw and rotate said first jaw toward said second jaw into a closed position, and wherein said lock system is configured to releasably hold said first jaw in said closed position; and

a firing member which is distinct from said closure member, wherein said firing member is actuated separately with respect to said closure member, wherein said firing member is responsive to said firing motion to deploy said staples from said staple cartridge, and wherein said firing member comprises a member configured to coact with one of said first jaw and said second jaw to set a jaw gap when said first jaw is in said closed position.

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专利名称(译)	外科缝合器械		
公开(公告)号	US9282966	公开(公告)日	2016-03-15
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[标]申请(专利权)人(译)	伊西康内外科公司		
申请(专利权)人(译)	爱惜康内镜手术，INC.		
当前申请(专利权)人(译)	爱惜康内镜手术，INC.		
[标]发明人	SHELTON IV FREDERICK E SETSER MICHAEL E WEISENBURGH II WILLIAM B		
发明人	SHELTON, IV, FREDERICK E. SETSER, MICHAEL E. WEISENBURGH, II, WILLIAM B.		
IPC分类号	A61B17/68 A61B17/64 A61B17/72 A61B17/10 A61B17/32 A61B18/14 A61B17/00 A61B17/29 A61B18/00 A61B17/068 A61B17/064 A61B17/072		
CPC分类号	A61B17/105 A61B17/064 A61B17/068 A61B17/0682 A61B17/072 A61B17/07207 A61B34/30 A61B50/20 A61B2017/00734 A61B2017/0688 A61B2017/07271 A61B2017/07278 A61B2017/2923 A61B2017/2927 A61B2017/320052 A61B2018/0063 A61B17/320092 A61B18/1445 A61B34/37 A61B2017/00017 A61B2017/00398 A61B2017/00473 A61B50/36 A61B2017/07285 A61B2018/00607 A61B2018/1455 A61B2090/0807 A61B2017/07257 A61B2017/320093 A61B2017/320094 A61B2017/320095 A61B2017/320097 A61B2034/302		
优先权	11/141753 2005-06-01 US 60/591694 2004-07-28 US		
其他公开文献	US20140151434A1		
外部链接	Espacenet USPTO		

摘要(译)

适用于腹腔镜和内窥镜临床手术的外科切断和缝合器械将组织夹在由砧座枢转地相对的细长通道的末端执行器内。电子束击发杆向远侧移动通过夹紧的末端执行器以切断组织并在切口的每一侧驱动钉。电子束击发杆肯定地将砧座与细长通道隔开，以确保适当形成的闭合钉，特别是当夹紧一定量的组织时，其不足以使端部执行器间隔开。特别地，击发杆的上销纵向移动通过砧座槽，并且通道槽被捕获在击发杆的下帽和中间销之间，以确保最小间距。从加厚的远端部分和变薄的近端条带形成电子束增强了可制造性并且便于在这种铰接手术器械中使用。

