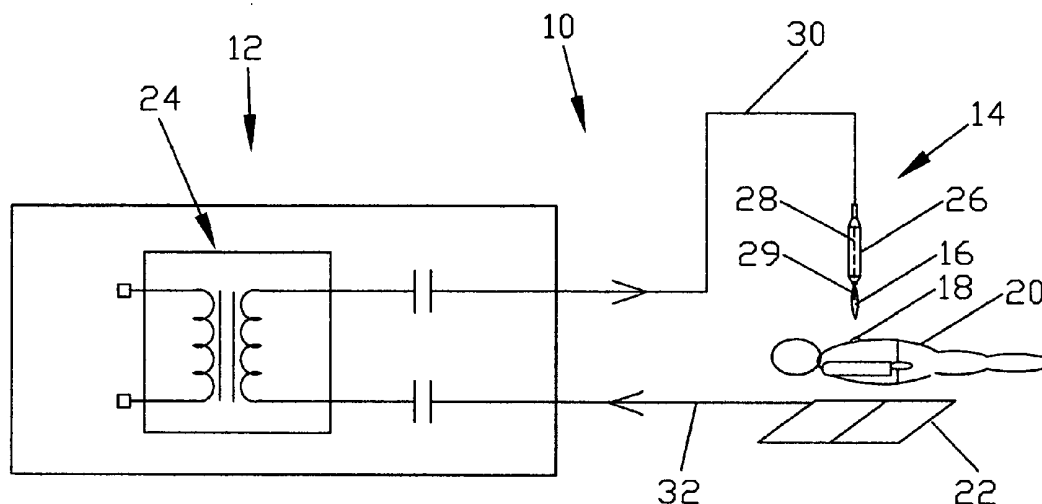




US 20120065635A1

(19) **United States**(12) **Patent Application Publication**
Konesky(10) **Pub. No.: US 2012/0065635 A1**(43) **Pub. Date: Mar. 15, 2012**(54) **ELECTROSURGICAL DEVICE TO
GENERATE A PLASMA STREAM****Publication Classification**(51) **Int. Cl.**
A61B 18/14 (2006.01)(52) **U.S. Cl.** **606/41**(57) **ABSTRACT**(75) **Inventor:** **Gregory A. Konesky**, Hampton
Bays, NY (US)(73) **Assignee:** **BOVIE MEDICAL
CORPORATION**, Clearwater, FL
(US)(21) **Appl. No.:** **13/295,261**(22) **Filed:** **Nov. 14, 2011****Related U.S. Application Data**(63) Continuation of application No. 12/006,680, filed on
Jan. 4, 2008, now Pat. No. 8,057,468, which is a con-
tinuation-in-part of application No. 10/321,947, filed
on Dec. 17, 2002, now Pat. No. 7,316,682.

An electrosurgical device to generate a plasma stream and method to perform endoscopic or laparoscopic surgery within a patient's body. The electrosurgical device includes an electrode operatively coupled to an electrosurgical generator to receive electrical energy therefrom, the electrode being concentrically disposed within an inner noble gas conduit to form a plasma channel. An outer electronegative gas conduit is disposed in surrounding coaxial relation relative to the inner noble gas conduit to cooperatively form an electronegative gas channel therebetween such that the electrode heats the noble gas to at least partially ionize the noble gas to generate the plasma stream to be directed to the surgical site to perform the surgical procedure while the electronegative gas sustains the plasma stream at the surgical site and dilutes the noble gas adjacent the surgical site. An outer aspiration conduit may be provided to remove fluid and solid debris from the surgical site.



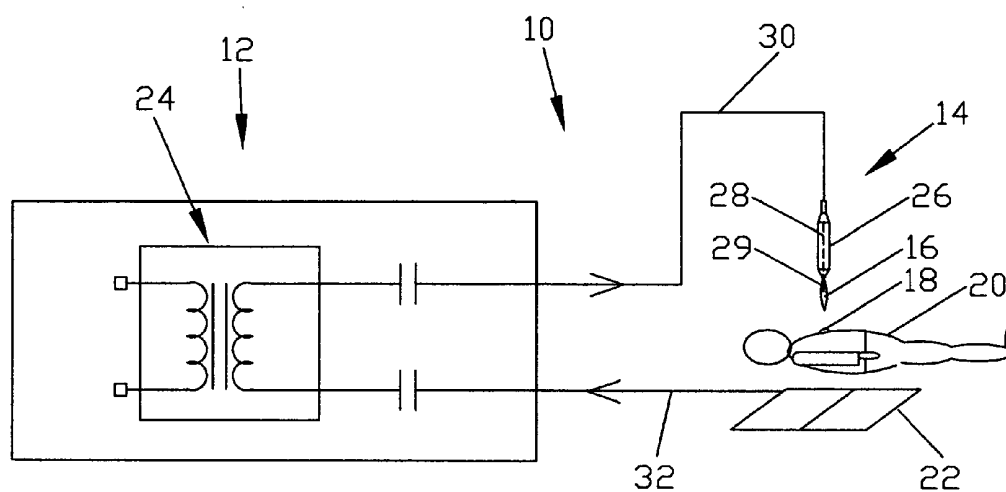


FIG. 1

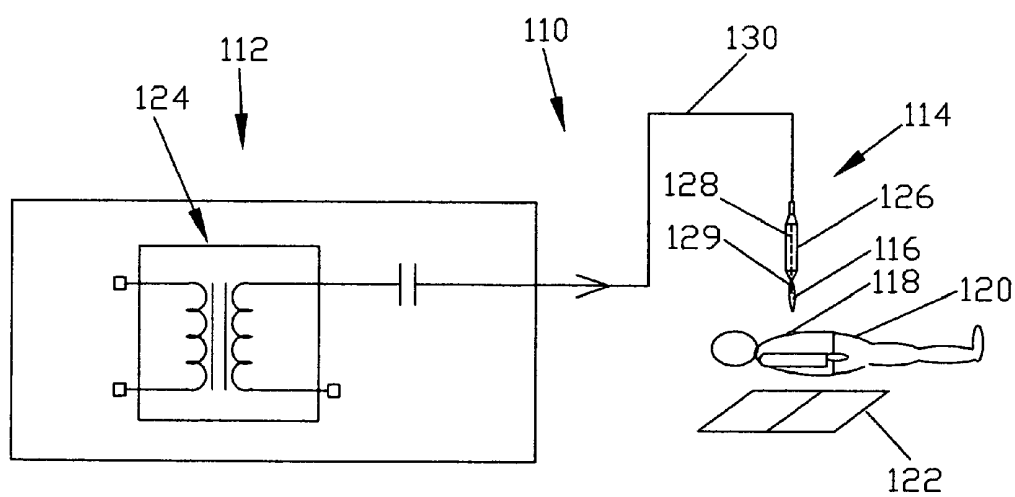


FIG. 2

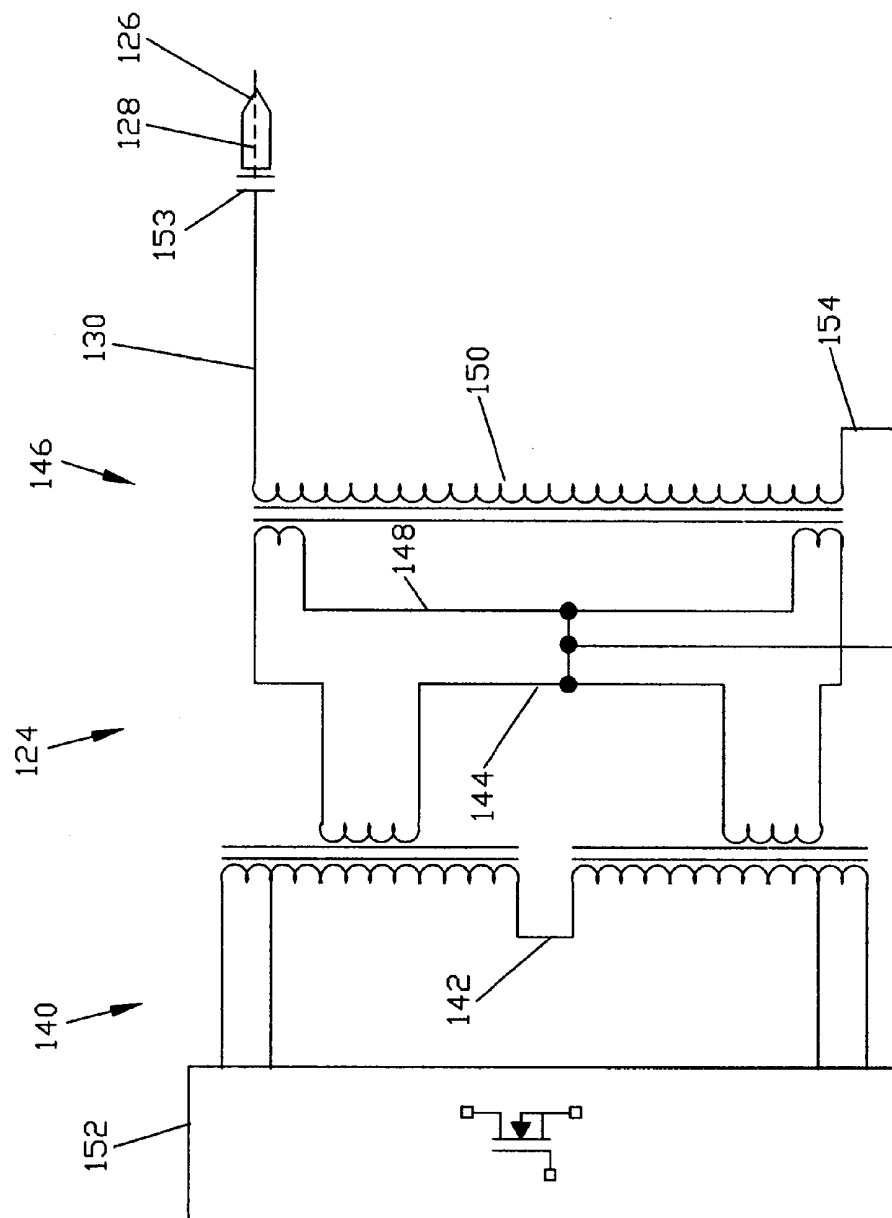
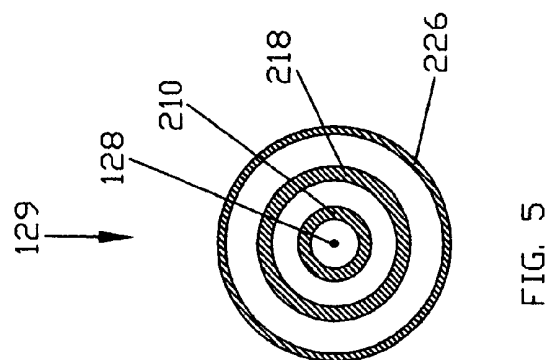
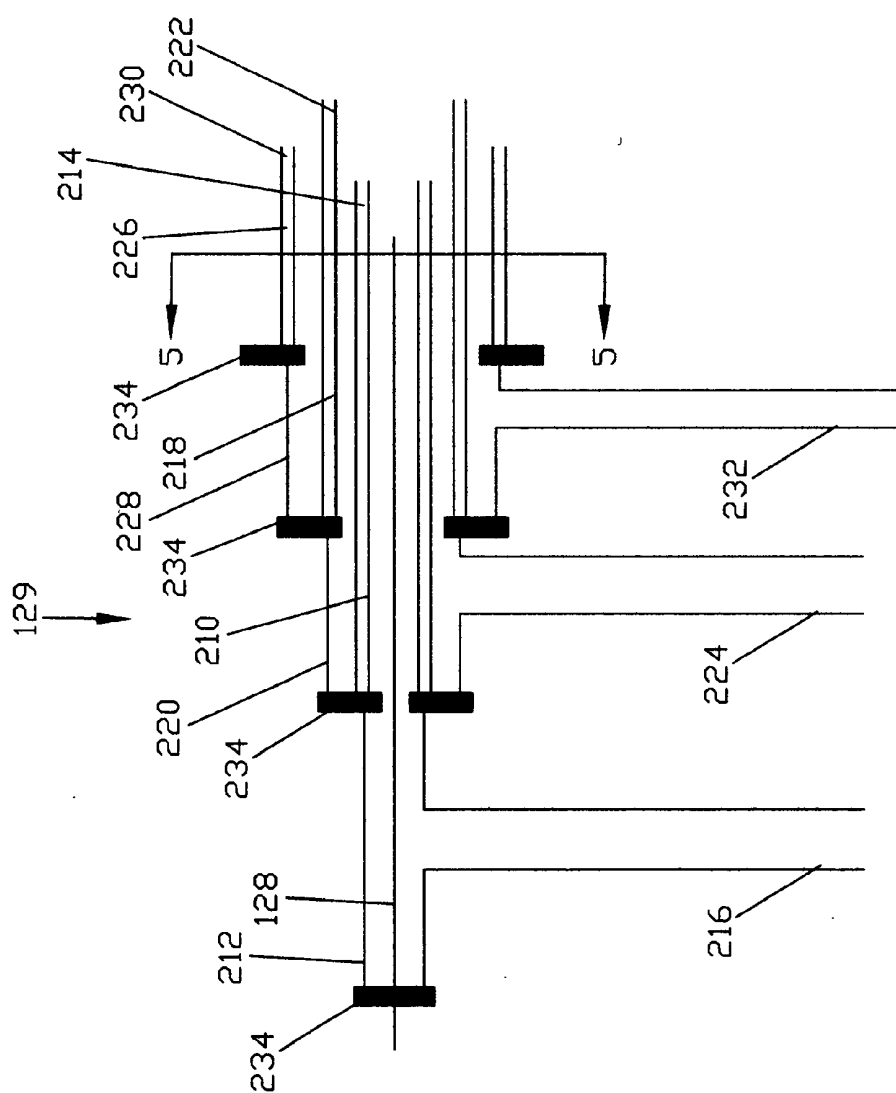


FIG. 3



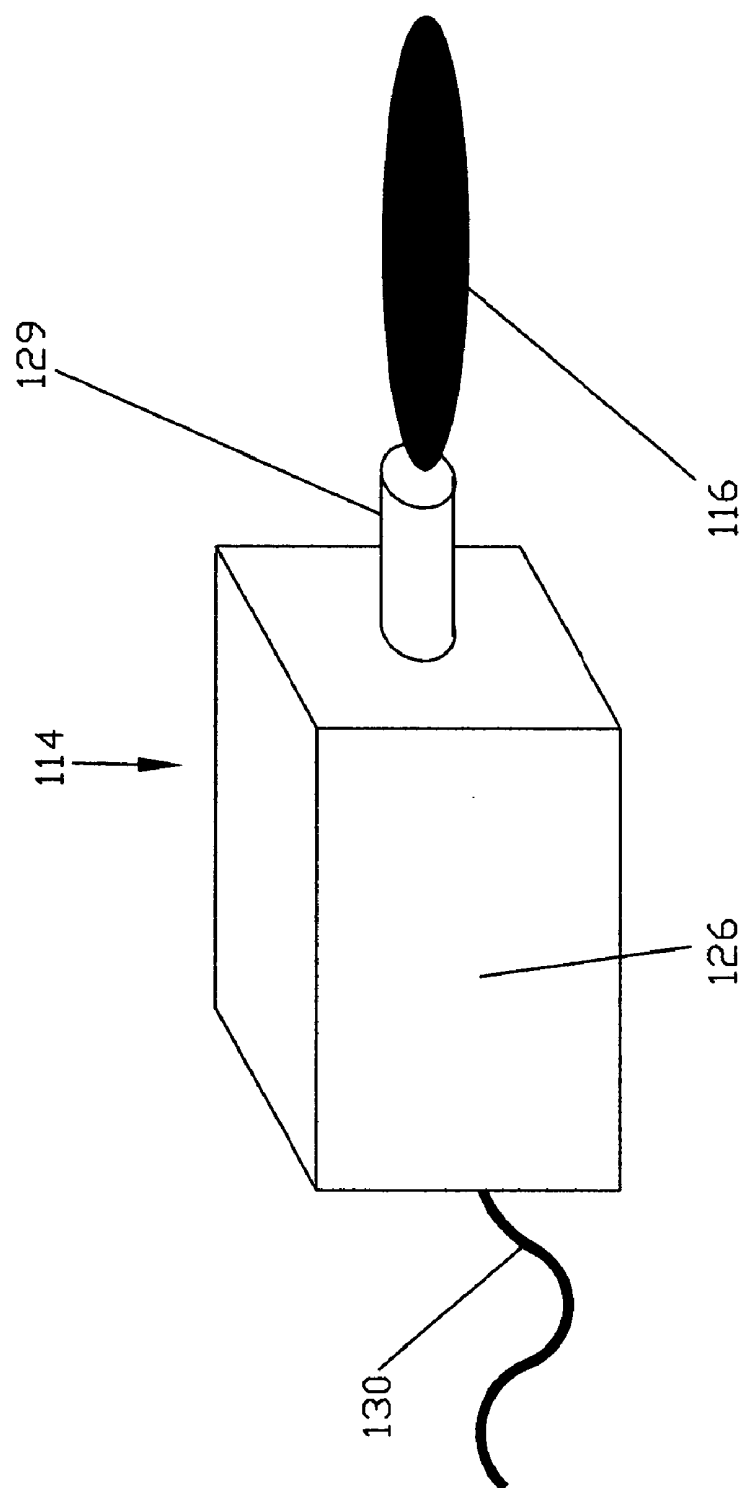


FIG. 6

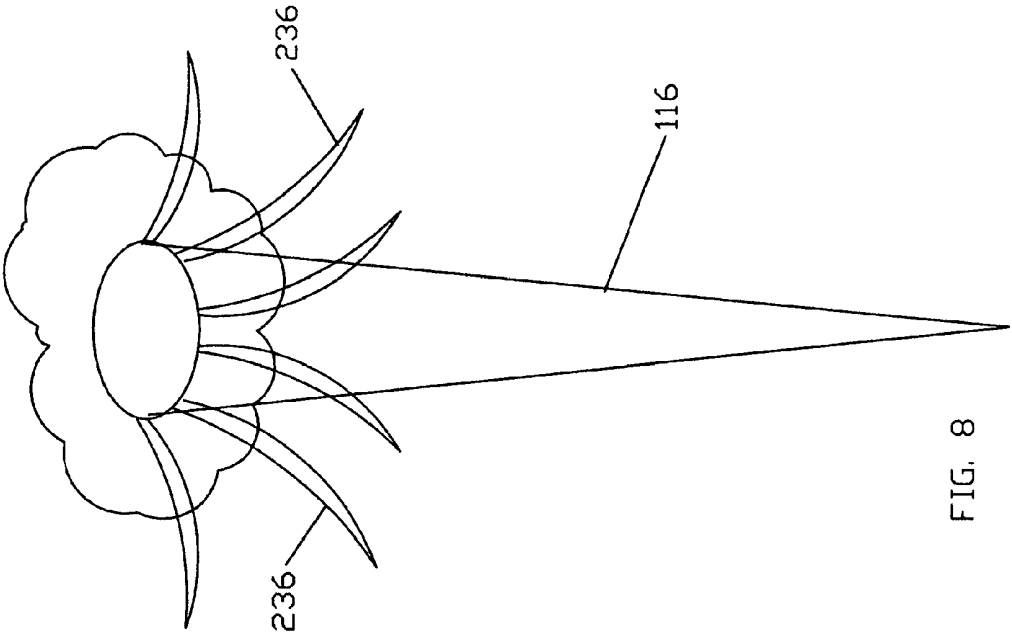


FIG. 8

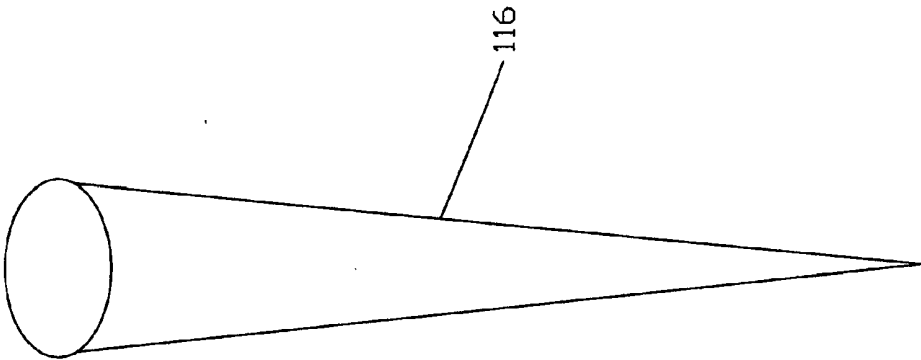


FIG. 7

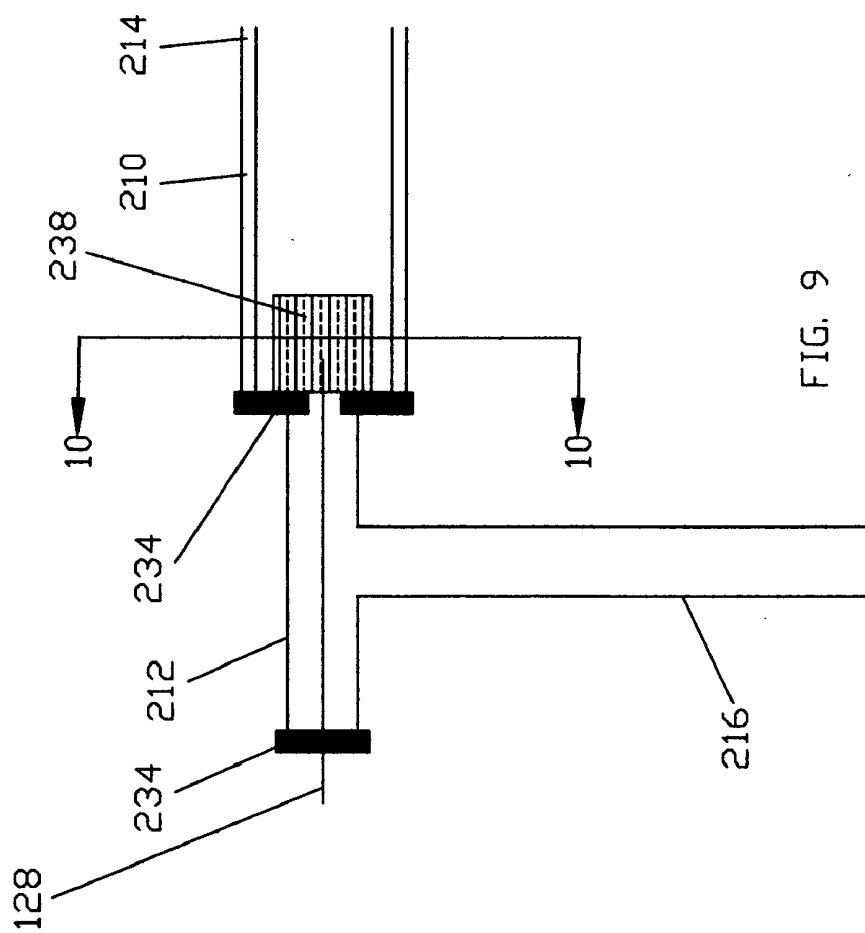


FIG. 9

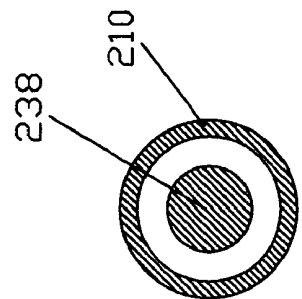


FIG. 10

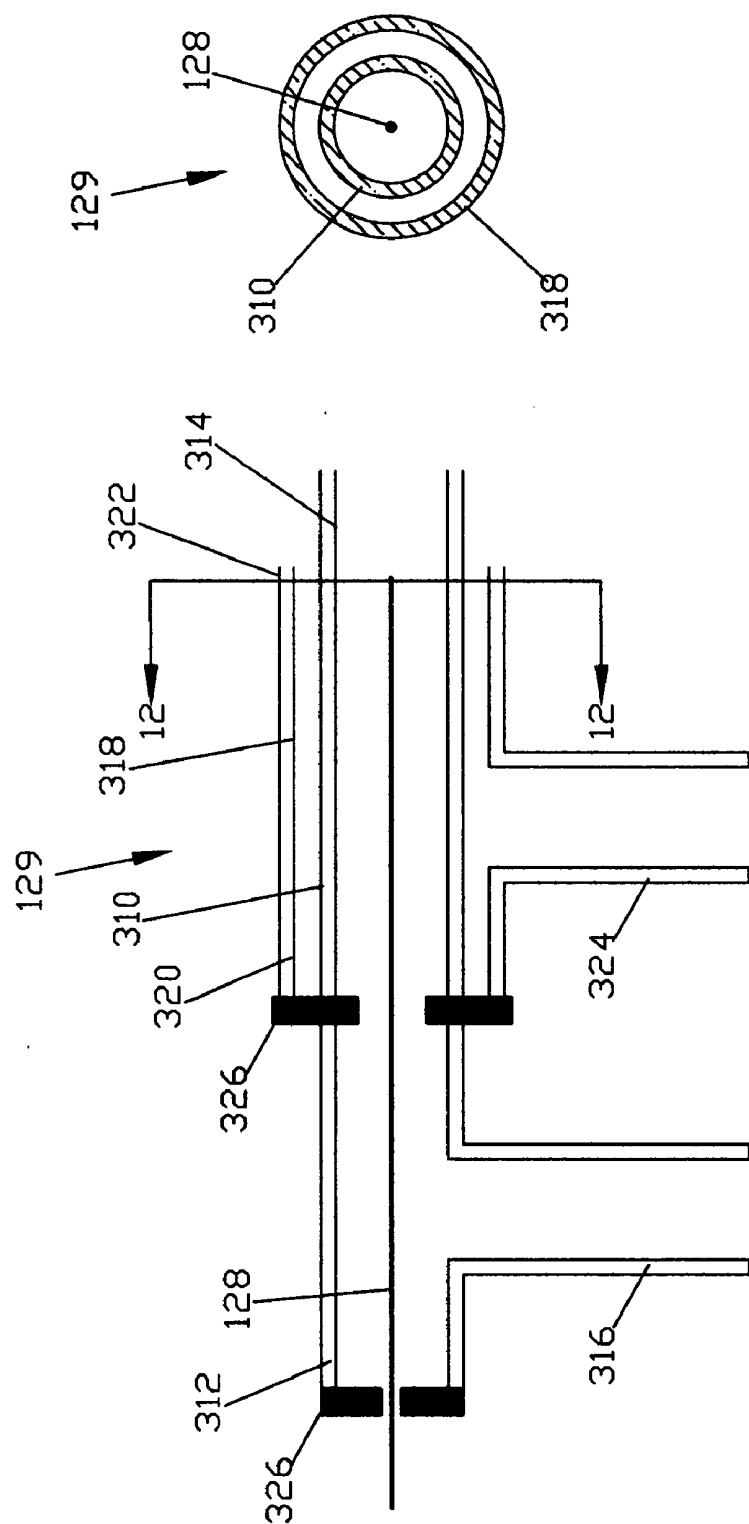


FIG. 12

FIG. 11

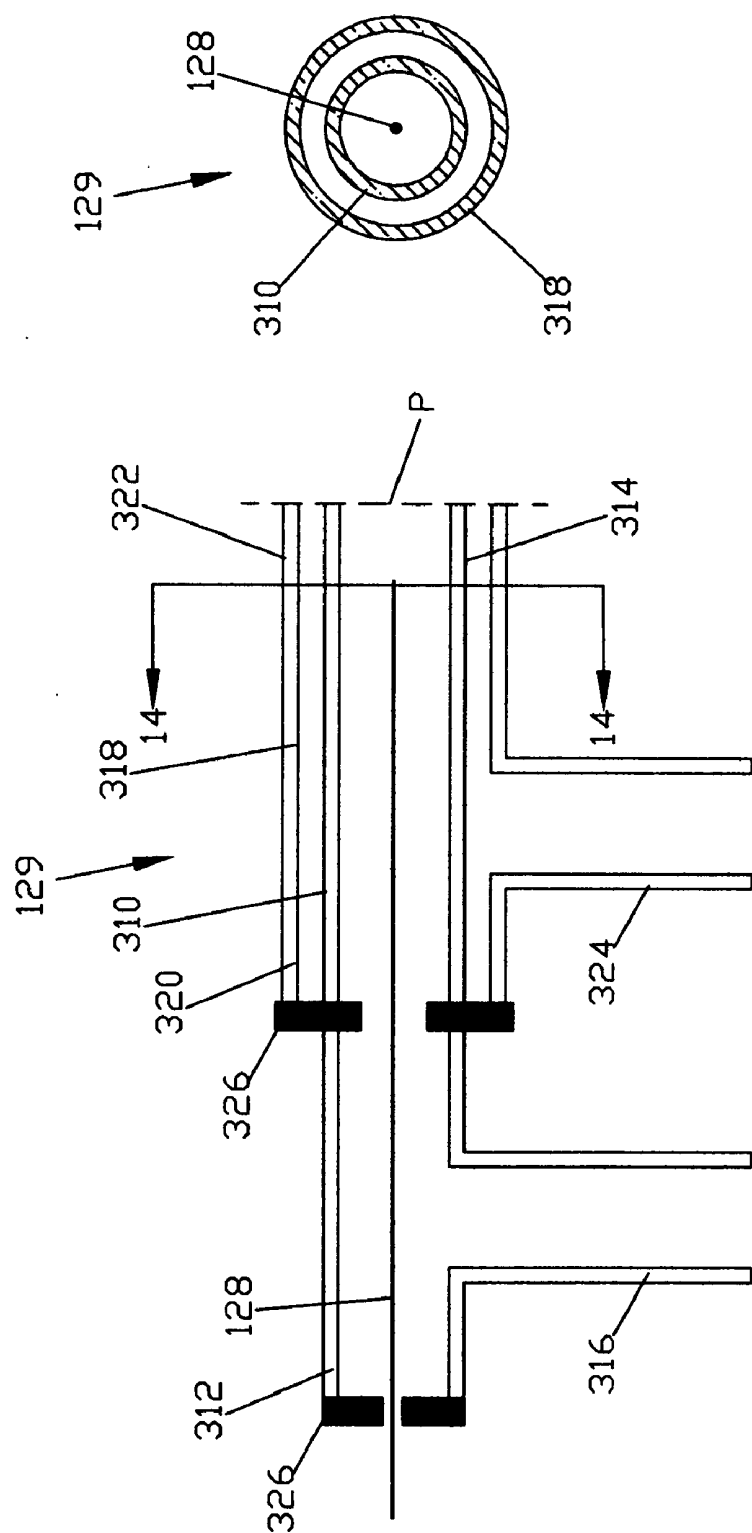


FIG. 14

FIG. 13

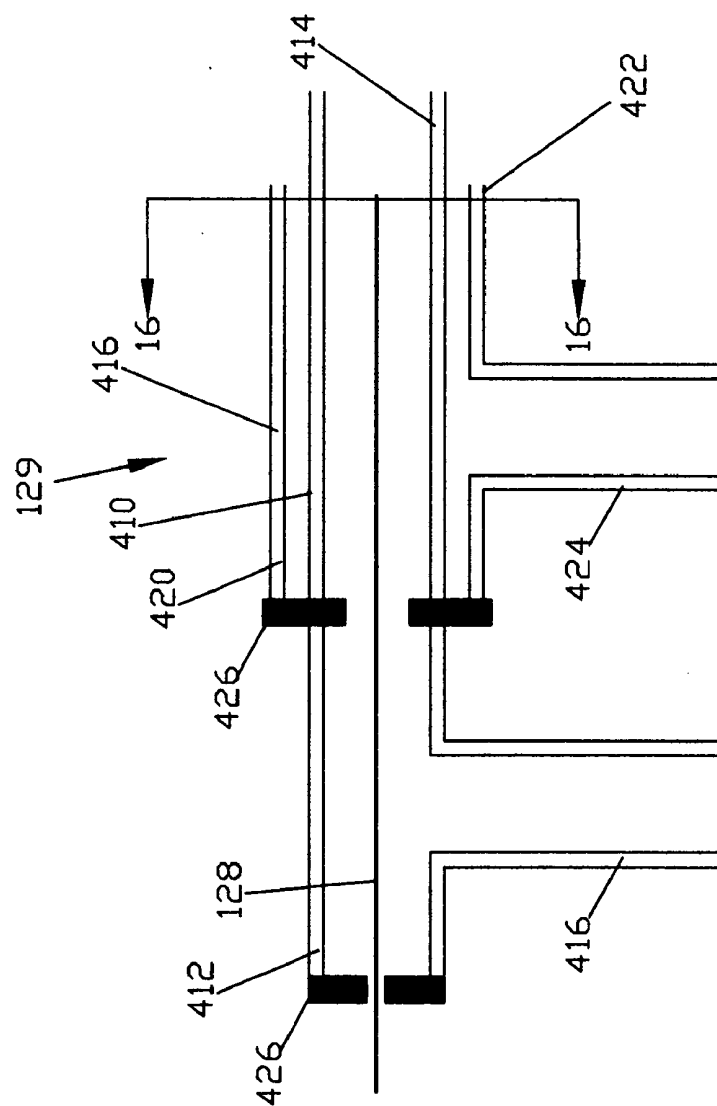


FIG. 15

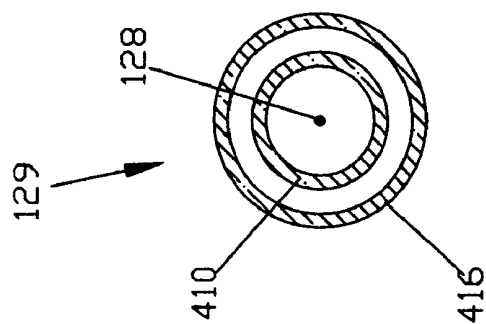


FIG. 16

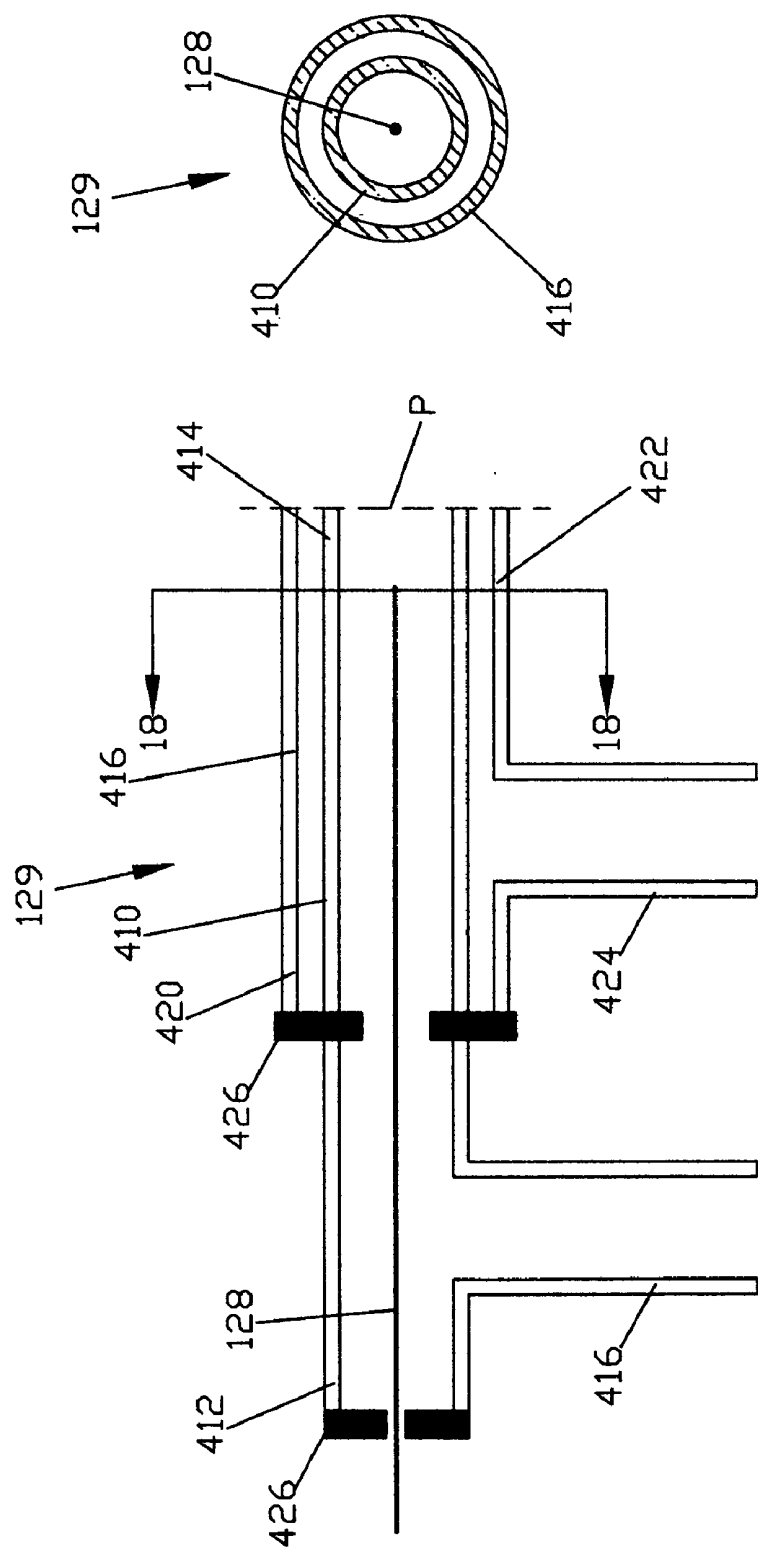


FIG. 17

FIG. 18

ELECTROSURGICAL DEVICE TO GENERATE A PLASMA STREAM

CROSS-REFERENCE

[0001] This application is a continuation application of copending application Ser. No. 12/006,680 filed on Jan. 4, 2008, which is a continuation-in-part application of application Ser. No. 10/321,947 filed on Dec. 17, 2002, now U.S. Pat. No. 7,316,682.

BACKGROUND OF THE INVENTION

[0002] 1. Field of the Invention

[0003] An electrosurgical device to generate a plasma stream and method to perform electrosurgery on a surgical target area on a patient.

[0004] 2. Description of the Prior Art

[0005] High frequency electrical energy has been widely used in surgery. Tissue is cut and bodily fluids are coagulated using electrosurgical energy.

[0006] Electrosurgical instruments generally comprise "monopolar" devices or "bipolar" devices. Monopolar devices comprise an active electrode on the electrosurgical instrument with a return electrode attached to the patient. In monopolar electrosurgery, the electrosurgical energy flows through the active electrode on the instrument through the patient's body to the return electrode. Such monopolar devices are effective in surgical procedures where cutting and coagulation of tissue are required and where stray electrical currents do not pose a substantial risk to the patient.

[0007] Bipolar devices comprise an active electrode and a return electrode on the surgical instrument. In a bipolar electrosurgical device, electrosurgical energy flows through the active electrode to the tissue of a patient through a short distance through the tissue to the return electrode. The electrosurgical effects are substantially localized to a small area of tissue that is disposed between the two electrodes on the surgical instrument. Bipolar electrosurgical devices have been found to be useful with surgical procedures where stray electrical currents may pose a hazard to the patient or where other procedural concerns require close proximity of the active and return electrodes. Surgical operations involving bipolar electrosurgery often require methods and procedures that differ substantially from the methods and procedures involving monopolar electrosurgery.

[0008] Gas plasma is an ionized gas capable of conducting electrical energy. Plasmas are used in surgical devices to conduct electrosurgical energy to a patient. The plasma conducts the energy by providing a pathway of relatively low electrical resistance. The electrosurgical energy will follow through the plasma to cut, coagulate, desiccate, or fulgurate blood or tissue of the patient. There is no physical contact required between an electrode and the tissue treated.

[0009] Electrosurgical systems that do not incorporate a source of regulated gas can ionize the ambient air between the active electrode and the patient. The plasma that is thereby created will conduct the electrosurgical energy to the patient, although the plasma arc will typically appear more spatially dispersed compared with systems that have a regulated flow of ionizable gas.

[0010] One of the difficulties in using a plasma is its initiation. A strong electrical field is required to accelerate enough free electrons within the gas such that a cascade of ionizing collisions is initiated which creates the plasma. This is some-

times called "igniting" the plasma. Once a plasma is ignited, it may be sustained at lower electrical field potentials.

[0011] Several techniques are presently used to create strong electrical fields that can ignite the plasma. One technique is to move the tip of an electrode very close to the surgical site. The electric field along a path between an electrode and the surgical site increases as their separation decreases, and may reach a level sufficient to ignite the plasma. The drawback of this method is that a surgeon must carefully manipulate the electrode to move it close to the surgical site without actually touching the tissue. If the electrode comes in contact with the tissue it may stick, causing eschar to deposit on the electrode. During laparoscopic procedures, it is often difficult for a surgeon to sense the proximity of the electrode to the tissue.

[0012] Another technique to ignite plasma is to use a pointed electrode which will generate a stronger electrical field at the tip of the electrode. However, a pointed electrode may be undesirable if the surgeon requires a blade-shaped electrode for cutting and other tissue manipulation. Yet another technique is to provide high voltage spikes to the surgical electrode until a detector has indicated a closed circuit with the return electrode. Once a closed circuit is detected, the high voltage spikes are terminated and the electrosurgical generator returns to its normal waveform output. While this technique is effective, it requires complicated electronics and components capable of withstanding the high voltages.

[0013] U.S. Pat. No. 4,060,088 relates to a monopolar electrosurgical method and apparatus for coagulation by fulguration. The apparatus has source of inert ionized gas which surrounds a tubular electrosurgical electrode. There is also disclosed a source of periodic bursts of electrosurgical energy used to initiate the plasma arc. Only one electrode is disclosed on the electrosurgical apparatus so that the device is monopolar.

[0014] U.S. Pat. No. 4,781,175 teaches the application of an ionizable gas jet to the tissue to clear bodily fluids and coagulate or achieve fulguration in the form of an improved eschar using an instrument having a conduit for the flow of gas at a predetermined flow rate about a centrally located electrode for electrosurgical energy. Circuitry and computer logic are shown to control the gas jet flow and the electrosurgical energy. No return path for the electrosurgical energy is provided.

[0015] U.S. Pat. No. 3,970,088, U.S. Pat. No. 3,987,795 and U.S. Pat. No. 4,043,342 describe sesquipolar electrodes on an instrument used to apply electrosurgical energy to an operative site.

[0016] U.S. Pat. No. 4,041,952 employs a switch on a forceps used as monopolar or bipolar during treatment of the patient with electrosurgery.

[0017] U.S. Pat. No. 4,890,610 discloses a pair of bipolar forceps comprising coined metallic conductive blades that are each over-molded with a plastic insulator to leave exposed tips at the patient end and connector terminals for electrosurgical energy at the opposite ends.

[0018] U.S. Pat. No. 4,492,231 teaches a bipolar circuit to provide non-stick coagulation by use of a good thermal conductor and minimal contact relative to the volume of conductive material in the tines of the forceps.

[0019] U.S. Pat. No. 4,060,088 relates to a monopolar electrosurgical unit in combination with an ionizable gas delivery system.

[0020] U.S. Pat. No. 4,040,426 shows a method and apparatus for initiating an electrical discharge in the ionizable gas.

[0021] U.S. Pat. No. 4,901,719 teaches a monopolar electrosurgical unit in combination with an ionizable gas delivery system including a gas conducting means.

[0022] U.S. Pat. No. 4,429,694 shows a solid-state electrosurgical generator which provides output waveforms that are optimized for electrosurgical fulguration. The fulguration output circuitry consists of a radio-frequency tank circuit which is periodically pulsed to produce a periodic damped-sinusoidal output waveform. However, the damping factor is sufficiently low so that many cycles of the waveform occur between periodic input pulses. Although the duty cycle is relatively high compared to prior art devices, cutting and burning effects are prevented by a high impedance output which internally limits fulguration arc current. The fulgurating arc developed by the device is longer and more consistent than that developed by previous devices thereby resulting in superior fulguration.

[0023] U.S. Pat. No. 4,901,720 discloses an electrosurgical generator in an electrosurgical unit (ESU) controls the repetition rate and the energy content of bursts of RF energy delivered to a gas jet supplied by the ESU, in order to maintain RF leakage current within acceptable limits while still achieving a sufficient state of ionization in the gas jet to reliably initiate the conduction of arcs to the tissue. The repetition rate of the RF bursts is substantially reduced in an inactive state when no arcs are delivered. A relatively small number of the RF bursts delivered during the inactive state have an increased or boosted energy content to assure an adequate ionization state in the gas jet.

[0024] U.S. Pat. No. 5,088,997 shows a device for enhancing the safety and efficiency of a hand-operated electrosurgical pencil having an electrode with a distal end defining a tip for cutting or coagulating biological tissue, which device comprises a nose piece adapted to be mounted about said electrode and containing conduit means defining converging pathways for streams of gas which impinge obliquely on said electrode at or near the tip thereof, and electrosurgical apparatus incorporating said device and a method for coagulating or cutting biological tissue using said apparatus.

[0025] U.S. Pat. No. 5,776,092 teaches an electrosurgical device including a noble gas channel and an aspiration channel coupled to a negative pressure source to remove fluid and solid debris from a surgical site disposed in side-by-side relationship.

[0026] U.S. Pat. No. 6,213,999 describes an apparatus and method for igniting plasma in a surgical system is disclosed. A corona discharge is generated on a surgical handpiece which is used to ignite a plasma arc for surgical operations. The advantages include greater reliability and repeatability of plasma arc ignition. The apparatus comprises a handpiece incorporating an active electrode, a passage for ionizable gas, and a corona return electrode. The corona return electrode has a terminus on the holder and near the distal end of the holder. The corona return electrode is electrically connected to the return path of the electrosurgical generator. A non-uniform electric field is generated between the active electrode and the corona return electrode of sufficient strength so that a corona is formed near the active electrode. A separate return electrode may be on the patient, or the apparatus may be configured for bipolar electrosurgical operation by carrying the return electrode on the handpiece. A dielectric material separates the active electrode and the corona return electrode.

There is substantially capacitive coupling between the active electrode and the corona return electrode. There is substantially resistive coupling between the active electrode and the return electrode.

[0027] Additional examples of the prior art are found in U.S. Pat. No. 1,889,609; U.S. Pat. No. 2,835,254; U.S. Pat. No. 3,577,030; U.S. Pat. No. 3,949,266; U.S. Pat. No. 4,559,943; U.S. Pat. No. 4,818,916; U.S. Pat. No. 4,887,005; U.S. Pat. No. 5,302,881; U.S. Pat. No. 5,325,019; U.S. Pat. No. 5,669,904; U.S. Pat. No. 5,710,486; U.S. Pat. No. 5,717,293; U.S. Pat. No. 5,801,489; U.S. Pat. No. 5,815,047; U.S. Pat. No. 5,917,286; U.S. Pat. No. 6,046,546; U.S. Pat. No. 6,181,068; U.S. Pat. No. 6,222,321; and U.S. Pat. No. 6,262,538.

SUMMARY OF THE INVENTION

[0028] The present invention relates to an electrosurgical device to generate a plasma stream to perform electrosurgery on a surgical site within a patient's body.

[0029] The electrosurgical device comprises an electrosurgical generator coupled to an electrical power source to supply power for the electrosurgical device and a plasma generator including an electrode operatively coupled to the electrosurgical generator to selectively receive electrical energy therefrom and to generate the plasma stream.

[0030] An inner noble gas conduit coupled to a noble gas source to feed noble gas such as helium or argon to the noble gas conduit surrounds the electrode to at least partially ionize the noble gas to create the plasma stream. An outer electronegative gas conduit disposed in surrounding coaxial relation relative to the inner noble gas conduit is coupled to a gas source to feed electronegative gas or air such as oxygen and/or nitrogen to the outer electronegative gas conduit to maintain the plasma stream at the surgical site and dilute the noble gas adjacent the surgical site to limit the area of the plasma stream to the surgical site. Alternately, an outer aspiration conduit coupled to a negative pressure source such as a vacuum is disposed in surrounding coaxial relation relative to the inner noble gas conduit to remove fluid and solid debris from the surgical site.

[0031] Oxygen and nitrogen in the atmosphere surrounding the plasma phase tend to act to confine the discharge to an elongated narrow beam. However, if plasma is applied to an internal cavity or endoscopically, the noble gas flow from the plasma stream displaces any air remaining within the cavity. In addition, the plasma stream is operated in a surrounding atmosphere, the plasma stream eventually discharges randomly. This is undesirable where precision pinpoint accuracy is required.

[0032] In order to maintain the profile of the plasma stream when used within a confined space, the outer electronegative gas conduit is employed.

[0033] Noble gas and air flow rates are generally equal. However, air flow rates in excess of the noble gas flow rate can be used to enhance flow-assisted removal of smoke and debris generated during the surgical procedure. Excessive flow rates of either noble gas or air can induce turbulence in the plasma stream and distort the discharge jet shape.

[0034] Gases other than air can be used in the outer electronegative gas conduit. Cross-boundary diffusion from the plasma stream into the surrounding air and air diffusion into the plasma stream limits the effective length of the plasma stream. By substituting additional noble gas flow for air in the outer electronegative gas conduit, a significantly extended plasma stream can be obtained. Reduced concentration gra-

dient occur with the noble gas from the inner ionized jet diffusing into non-ionized noble gas in the outer coaxial flow and vice versa. This results in overall plasma stream that are between two and two and a half times as long as those without a coaxial noble gas flow under otherwise identical conditions.

[0035] Since the cross section area of a conduit scales with the square of the radius, the diameter of the outer aspiration conduit need not be excessive to accommodate the inner noble gas conduit. At the same time, the inside diameter of the outer aspiration conduit should be large enough to permit aspiration of fluid and debris generated during the surgical procedure.

[0036] Saline solution may be intermittently substituted for the air flow to enhance debris removal. Plasma activation should be suspended during this phase or mode of the procedure.

[0037] The invention accordingly comprises the features of construction, combination of elements, and arrangement of parts that will be exemplified in the construction hereinafter set forth, and the scope of the invention will be indicated in the claims.

BRIEF DESCRIPTION OF THE DRAWINGS

[0038] For a fuller understanding of the nature and object of the invention, reference should be had to the following detailed description taken in connection with the accompanying drawings in which:

[0039] FIG. 1 is a schematic of a monopolar electrosurgical device and a patient.

[0040] FIG. 2 is a schematic of the electrosurgical device of the present invention and a patient.

[0041] FIG. 3 is a detailed schematic of the isolated, non-floating transformer of the electrosurgical generator of the electrosurgical device of the present invention.

[0042] FIG. 4 is a partial diagrammatic side view of the plasma generator of the electrosurgical device of the present invention.

[0043] FIG. 5 is a cross sectional end view of the plasma generator of the electrosurgical device of the present taken along line 5-5 of FIG. 4.

[0044] FIG. 6 is a perspective view of the plasma generator of the electrosurgical device of the present invention.

[0045] FIG. 7 depicts a plasma stream in an ambient atmosphere.

[0046] FIG. 8 depicts a plasma stream in a helium atmosphere.

[0047] FIG. 9 is a partial diagrammatic side view of an alternate embodiment of the plasma generator of the electrosurgical device of the present invention.

[0048] FIG. 10 is a cross sectional end view of the alternate embodiment of the plasma generator of the electrosurgical device of the present invention taken along line 10-10 of FIG. 9.

[0049] FIG. 11 is a partial diagrammatic side view of another alternate embodiment of the plasma generator of the electrosurgical device of the present invention.

[0050] FIG. 12 is a cross sectional end view of the alternate embodiment of the plasma generator of the electrosurgical device of the present taken along line 12-12 of FIG. 11.

[0051] FIG. 13 is a partial diagrammatic side view of yet another alternate embodiment of the plasma generator of the electrosurgical device of the present invention.

[0052] FIG. 14 is a cross sectional end view of the alternate embodiment of the plasma generator of the electrosurgical device of the present invention taken along line 14-14 of FIG. 13.

[0053] FIG. 15 is a partial diagrammatic side view of still another alternate embodiment of the plasma generator of the electrosurgical device of the present invention.

[0054] FIG. 16 is a cross sectional end view of the alternate embodiment of the plasma generator of the electrosurgical device of the present taken along line 16-16 of FIG. 15.

[0055] FIG. 17 is a partial diagrammatic side view of still yet another alternate embodiment of the plasma generator of the electrosurgical device of the present invention.

[0056] FIG. 18 is a cross sectional end view of the alternate embodiment of the plasma generator of the electrosurgical device of the present invention taken along line 18-18 of FIG. 17.

[0057] Similar reference characters refer to similar parts throughout the several views of the drawings.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENT

[0058] The present invention relates to an electrosurgical device and method of use in endoscopic and laparoscopic surgery. As described more fully hereinafter, the electrosurgical device comprises an electrosurgical generator to supply power to the electrosurgical device and a plasma generator operatively coupled to the electrosurgical generator to receive electrical power therefrom and to generate a plasma stream for application to a surgical site or target area on a patient.

[0059] FIG. 1 shows a prior art monopolar electrosurgical device generally indicated as 10 comprising an electrosurgical generator generally indicated as 12 to generate power for the electrosurgical device 10 and a plasma generator generally indicated as 14 to generate and apply a plasma stream 16 to a surgical site or target area 18 on a patient 20 resting on a conductive plate or support surface 22.

[0060] The electrosurgical generator 12 includes a transformer generally indicated as 24 including a primary and secondary coupled to an electrical source (not shown) to provide high frequency electrical energy to the plasma generator 14. Typically, the electrosurgical generator 12 comprises an isolated floating potential not referenced to any potential. Thus, current flows between the active and return electrodes. If the output is not isolated, but referenced to "earth", current can flow to areas with ground potential. If the contact surface of these areas and the patient is relatively small, an undesirable burning can occur.

[0061] The plasma generator 14 comprises a handpiece or holder 26 having an electrode 28 at least partially disposed within a fluid flow housing 29 and coupled to the transformer 24 to receive the high frequency electrical energy therefrom to at least partially ionize noble gas fed to the fluid flow housing 29 of the handpiece or holder 26 to generate or create the plasma stream 16.

[0062] The high frequency electrical energy is fed from the secondary of the transformer 24 through an active conductor 30 to the electrode 28 (collectively active electrode) in the handpiece 26 to create the plasma stream 16 for application to the surgical site 18 on the patient 20.

[0063] The return path to the electrosurgical generator 12 is through the tissue and body fluid of the patient 20, the conductor plate or support member 22 and a return conductor 32

(collectively return electrode) to the secondary of the transformer **24** to complete the isolated, floating potential circuit.

[0064] U.S. Pat. No. 6,213,999 discloses both monopolar and bipolar electrosurgical generators.

[0065] As shown in FIG. 2, the electrosurgical device **110** of the present invention comprises an electrosurgical generator generally indicated as **112** to generate power for the electrosurgical device **110** and a plasma generator **114** to generate and apply a plasma stream **116** to a surgical site or target area **118** on a patient **120** resting on a conductive plate or support element **122**.

[0066] The electrosurgical generator **112** includes a transformer generally indicated as **124** including a primary and secondary coupled to an electrical source (not shown) to provide high frequency electrical energy to the plasma generator **114**. Typically, the electrosurgical generator **112** comprises an isolated nonfloating potential not referenced to any potential.

[0067] The plasma generator **114** comprises a handpiece or holder **126** having an electrode **128** at least partially disposed within a fluid flow housing **129** and coupled to the transformer **124** to receive the high frequency electrical energy therefrom to at least partially ionize noble gas fed to the fluid flow housing **129** of the handpiece or holder **126** to generate or create the plasma stream **116**.

[0068] The high frequency electrical energy is fed from the secondary of the transformer **124** through an active conductor **130** to the electrode **128** in the handpiece **126** to create the plasma stream **116** for application to the surgical site **118** on the patient **120**.

[0069] The plasma current flow back to the electrosurgical generator **112** is through the tissue and body fluid and the patient **120**. From there, the return current circuit is completed through the combined external capacitance to the plasma generator handpiece **124**, surgeon and through displacement current in the air. The capacitance is determined, among other things, by the physical size of the patient **120**.

[0070] FIG. 3 shows the transformer **124** in detail. The transformer **124** comprises a step-down section or stage generally indicated as **140** including a primary **142** and secondary **144** and a step-up section or stage generally indicated as **146** including a primary **148** and secondary **150** operatively coupled together. The primary **142** of the step-down section or stage **140** is coupled across a power amplifier **152**; while, the secondary **150** of the step-up section or stage **146** is coupled between the electrode **128** through the active conductor **130** and a series capacitor **153** and the isolated non-floating return **154**. The step-down, step-up configuration provides a fixed or constant potential (FIXEDPOT).

[0071] The series capacitor **153** is equal to or less than 20 pF limiting the leakage current to a safe level below about 150 mA RMS. Compared to a typical load of from about fifty ohms, the Z_c is relatively high. As a result, the current output of the plasma generator **114** is substantially constant. In addition, the transformer output has a substantial constant potential. The continuous output waveform has a crest factor of about 1.4-1.5. As a result, the ignition of the noble gas is relatively stable.

[0072] Thus, the plasma output is a relatively constant current source and the working currents do not exceed about 150 mA RMS. Here the leakage current is the functional current. Because the value of the current and crest-factor is low, but V_{pp} voltage—very high, the heat transfer in the tissue is very

low, so undesired tissue damage is very low. Increasing the application time could compensate the insufficient heat transfer.

[0073] The plasma generator effect also depends on the shape of the electrode. If the electro-magnetic field in the “near zone” around the electrode tip is constant compared with the electromagnetic wave length (400 kHz), the EMF can be considered static. In that case, the ignition of the plasma depends on the so-called “electrostatic pressure”, which is higher for sharper electrode shapes. Thus, the sharper and thinner the electrode is, the better initial (cold) plasma ignition. After the cold ignition the plasma beam is supported by the thermo electronic emission, which, due to the low current, is not as intensive as in the APC.

[0074] As best shown in FIGS. 4 and 5, the plasma generator **114** includes the electrode **128** supported by the handpiece **126** and at least partially disposed in the fluid flow housing **129**. As previously described, the electrode **128** is operatively coupled to the electrosurgical generator **112** to selectively receive electrical energy therefrom. The electrode **128** is concentrically disposed within an inner noble gas conduit **210** having a proximal end **212** and a distal end **214** coupled to a noble gas source (not shown) by a noble gas supply conduit **216** to feed noble gas such as helium or argon to the noble gas conduit **210**.

[0075] An intermediate air or electronegative gas conduit **218** is disposed in surrounding coaxial relation relative to the noble gas conduit **210** having a proximal end **220** and a distal end **222** coupled to a gas source (not shown) by an air or electronegative gas supply conduit **224** to feed air or electronegative gas such as oxygen and nitrogen to the intermediate air or electronegative gas conduit **218**. The distal end **214** of the inner noble gas conduit **210** is disposed inwardly from the distal end **222** of the intermediate electronegative gas conduit **218**. Alternately, in place of the air or electronegative gas, noble gas may be fed through the intermediate air or electronegative gas conduit **218** to create a diffuse cylindrically shaped relatively wide area plasma beam useful with particular procedures such as dermatology.

[0076] An outer aspiration conduit **226** is disposed in surrounding coaxial relation relative to the intermediate air or electronegative gas conduit **218** having a proximal end **228** and a distal end **230** coupled to a negative pressure source such as a vacuum (not shown) by a negative pressure conduit **232** to remove fluid and solid debris from the target area **118** on the patient **120**. The distal end **230** of the outer aspiration conduit **226** is disposed inwardly from the distal end **222** of the intermediate air or electronegative gas conduit **218**.

[0077] A plurality of seals each indicated as **234** are used to seal the noble gas conduit **210**, the intermediate air or electronegative gas conduit **218** and the outer aspiration gas conduit **226**.

[0078] FIGS. 9 and 10 show an alternate embodiment of the plasma generator **114** including the electrode **128** supported by the handpiece **126** and at least partially disposed in the fluid flow housing **129**. The electrode **128** is concentrically disposed within the inner noble gas conduit **210** having a proximal end **212** and a distal end **214** coupled to a noble gas source (not shown) by a noble gas supply conduit **216** to feed noble gas such as helium or argon to the noble gas conduit **210**. A sintered conductive element **238** is disposed on the distal portion of the electrode **128** at least partially disposed within the inner noble gas conduit **210**.

[0079] In use, the electrosurgical device 110 is effective and safe in various applications such as open surgery, skin resurfacing, sterilization and internal surgery.

[0080] There are two operating modes, a gentle mode and an aggressive mode. The mechanisms for energy delivered to the surgical site 118 for the two modes are different. It was found that energy is delivered either through volumetric heating or surface heating.

[0081] In volumetric heating, the energy flux is distributed within the target volume. In this mechanism, the discharge current dissipates energy in the target material.

[0082] Surface heating can be defined as heating due to hot gas flow and heating due to direct heating by the high temperature plasma stream 116 in contact with the target area 118.

[0083] In the gentle mode, a jet of hot gas is generated. Very small current is induced through the plasma stream 116, and the plasma is created in a regime of electric field induced breakdown of the gas, such as in a fluorescent lamp. Energy deposition to the patient 120 is mostly through a flux of heated gas. A small current of less than about 250 .mu.A RMS, flows through the patient 120. It takes about 0.25 seconds for the noble gas discharge to reach a stable equilibrium flow rate of about 0.05 second in the gentle mode.

[0084] In the aggressive mode, preferred for surgical applications, a relatively high current is induced in the plasma stream 116, substantially increasing the temperature and density. As previously stated, the return current flows back to the electrosurgical generator 112 through the patient/target, and from there through the surrounding air and the surgeon holding the handpiece 126. Energy deposition to the patient 120 in this mode of operation is mostly electrical, through charged particle bombardment of the patient/target. The conducting plasma stream 116 couples the electrosurgical generator 112 to the patient 120. Peak patient/target currents as high as about 200 mA are generated. The value of this current is inversely proportional to the distance between the patient 120 and the handpiece 126.

[0085] The noble gas flow from the plasma generator nozzle 129 is laminar creating a stable gas flow and a focused plasma stream 116 as shown in FIGS. 6 through 8. The laminar flow protects the plasma stream 116 from penetration of oxygen and nitrogen which are electronegative and abundant in the surrounding air thereby preserving the stability of the focused plasma stream 116 of being quenched by the air or oxygen/nitrogen.

[0086] The thin, focused, plasma stream 116 acts as an extended, non-contact electrode, which delivers the current to the exposed surface of the target area 118. This primary arc induces multiple secondary sparks on a large area of the target area 118 and are capable of evaporating target tissue much like an electrosurgical ablation probe. Both the primary arc 116 and the multiple secondary sparks 236 are shown in FIG. 8. The multiple secondary sparks 236 can gradually remove material away from the primary arc 116. In other words, the area affected by the plasma generator stream is larger than the cross sectional area of the primary plasma stream 116.

[0087] The plasma stream current is a function of the drive capabilities of the electrosurgical generator 112 as well as the total impedance of the return current loop including the displacement current area. The smaller the capacitance and the conductivity from the patient 120 to the ground electrode of the transformer 124, the smaller is the current flowing

through the return current circuit. The plasma stream current is limited by the generator rating or the return current path whichever is smaller.

[0088] FIGS. 11 and 12 show an alternate embodiment of the plasma generator 114 including the electrode 128 at least partially disposed in the fluid flow housing 129. As previously described, the electrode 128 is operatively coupled to the electrosurgical generator 112 to selectively receive electrical energy therefrom. The electrode 128 is concentrically disposed within an inner noble gas conduit 310 having a proximal end 312 and a distal end 314 coupled to a noble gas source (not shown) by a noble gas supply conduit 316 to feed noble gas such as helium or argon to the inner noble gas conduit 310.

[0089] An outer air or electronegative gas conduit 318 is disposed in surrounding coaxial relation relative to the inner noble gas conduit 310 having a proximal end 320 and a distal end 322 coupled to a gas source (not shown) by an air or electronegative gas supply conduit 324 to feed air or electronegative gas such as oxygen and nitrogen to the outer air or electronegative gas conduit 318. The distal end 314 of the inner noble gas conduit 310 is disposed outwardly from the distal end 322 of the outer air or electronegative gas conduit 318.

[0090] A plurality of seals each indicated as 326 are used to seal the inner noble gas conduit 310 and the outer air or electronegative gas conduit 318.

[0091] FIGS. 13 and 14 show another embodiment of the plasma generator 114 including the electrode 128 at least partially disposed in the fluid flow housing 129 similar to the embodiment shown in FIGS. 11 and 12. As previously described, the electrode 128 is operatively coupled to the electrosurgical generator 112 to selectively receive electrical energy therefrom. The electrode 128 is concentrically disposed within an inner noble gas conduit 310 having a proximal end 312 and a distal end 314 coupled to a noble gas source (not shown) by a noble gas supply conduit 316 to feed noble gas such as helium or argon to the inner noble gas conduit 310.

[0092] An outer air or electronegative gas conduit 318 is disposed in surrounding coaxial relation relative to the inner noble gas conduit 310 having a proximal end 320 and a distal end 322 coupled to a gas source (not shown) by an air or electronegative gas supply conduit 324 to feed air or electronegative gas such as oxygen and nitrogen to the outer air or electronegative gas conduit 318. The distal end 314 of the inner noble gas conduit 310 is disposed in substantially the same plane P, substantially perpendicular to the longitudinal axis of the electrode 128, as the distal end 322 of the outer air or electronegative gas conduit 318.

[0093] A plurality of seals each indicated as 326 are used to seal the inner noble gas conduit 310 and the outer air or electronegative gas conduit 318.

[0094] Since the air or electronegative gas dilutes the noble gas adjacent the surgical site, the concentration of noble gas away from the surgical site 118 within the patient is diluted and therefore will not continue to be ionized.

[0095] FIGS. 15 and 16 show yet another plasma generator 114 including the electrode 128 at least partially disposed in the fluid flow housing 129 similar to the embodiment shown in FIGS. 11 and 12. As previously described, the electrode 128 is operatively coupled to the electrosurgical generator 112 to selectively receive electrical energy therefrom. The electrode 128 is concentrically disposed within an inner noble

gas conduit **410** having a proximal end **412** and a distal end **414** coupled to a noble gas source (not shown) by a noble gas supply conduit **416** to feed noble gas such as helium or argon to the inner noble gas conduit **410**.

[0096] An outer aspiration conduit **418** is disposed in surrounding coaxial relation relative to the inner noble gas conduit **410** having a proximal end **420** and a distal end **422** coupled to a negative pressure source such as a vacuum (not shown) by a negative pressure conduit **424** to remove fluid and solid debris from the target area **118** within the patient **120**. The distal end **422** of the outer aspiration conduit **418** is disposed inwardly from the distal end **414** of the inner noble gas conduit **410**.

[0097] A plurality of seals each indicated as **426** are used to seal the inner noble gas conduit **410** and the outer aspiration gas conduit **418**.

[0098] FIGS. 17 and 18 show still yet another plasma generator **114** including the electrode **128** at least partially disposed in the fluid flow housing **129** similar to the embodiment shown in FIGS. 15 and 16. As previously described, the electrode **128** is operatively coupled to the electrosurgical generator **112** to selectively receive electrical energy therefrom. The electrode **128** is concentrically disposed within an inner noble gas conduit **410** having a proximal end **412** and a distal end **414** coupled to a noble gas source (not shown) by a noble gas supply conduit **416** to feed noble gas such as helium or argon to the inner noble gas conduit **410**.

[0099] An outer aspiration conduit **418** is disposed in surrounding coaxial relation relative to the inner noble gas conduit **410** having a proximal end **420** and a distal end **422** coupled to a negative pressure source such as a vacuum (not shown) by a negative pressure conduit **424** to remove fluid and solid debris from the target area **118** within the patient **120**. The distal end **422** of the outer aspiration conduit **418** is disposed substantially in the same plane P, substantially perpendicular to the longitudinal axis of the electrode **128**, as the distal end **414** of the inner noble gas conduit **410**.

[0100] A plurality of seals each indicated as **426** are used to seal the inner noble gas conduit **410** and the outer aspiration gas conduit **418**.

[0101] It will thus be seen that the objects set forth above, among those made apparent from the preceding description are efficiently attained and since certain changes may be made in the above construction without departing from the scope of the invention, it is intended that all matter contained in the above description or shown in the accompanying drawing shall be interpreted as illustrative and not in a limiting sense.

[0102] It is also to be understood that the following claims are intended to cover all of the generic and specific features of the invention herein described, and all statements of the scope of the invention which, as a matter of language, might be said to fall therebetween.

[0103] Now that the invention has been described,

What is claimed is:

1. An electrosurgical handpiece to generate a plasma stream for performing electrosurgery on a surgical site on a patient comprising:

an electrode configured to be operatively coupled to an electrosurgical generator to receive electrical energy therefrom and disposed within an inner noble gas conduit;

said inner noble gas conduit including a distal end and a proximal end to form a plasma channel, said inner noble

gas conduit configured to be operatively coupled to a noble gas source to feed noble gas to said inner noble gas conduit such that said electrode at least partially ionizes the noble gas to generate the plasma stream to be directed to the surgical site to perform the surgical procedure; and

an intermediate electronegative gas conduit including a distal end and a proximal end disposed in surrounding relation relative to said inner noble gas conduit to cooperatively form an electronegative gas channel therebetween, said intermediate electronegative gas conduit configured to be operatively coupled to a gas source to feed electronegative gas to said electronegative gas channel, said distal end of said intermediate electronegative gas conduit extending beyond said distal end of said inner noble gas conduit such that the electronegative gas sustains the plasma stream.

2. The electrosurgical handpiece of claim 1, further including an outer aspiration conduit disposed in surrounding relation relative to said intermediate electronegative gas conduit to cooperatively form an aspiration channel therebetween coupled to a negative pressure source, said negative pressure source to remove fluid and solid debris from said surgical site.

3. The electrosurgical handpiece of claim 2, wherein said intermediate electronegative gas conduit is further configured to be coupled to a saline solution source for intermittently substituting a saline solution for the electronegative gas to enhance debris removal.

4. The electrosurgical handpiece of claim 1, wherein said intermediate gas conduit is coupled to a second noble gas source to feed noble gas to the electronegative gas channel to form a secondary plasma stream to at least partially envelop said plasma stream to at least partially ionize the secondary plasma stream.

5. An electrosurgical handpiece to generate a plasma stream for performing electrosurgery on a surgical site on a patient comprising:

an electrode configured to be operatively coupled to an electrosurgical generator to receive electrical energy therefrom and disposed within an inner noble gas conduit;

said inner noble gas conduit including a distal end and a proximal end to form a plasma channel, said inner noble gas conduit configured to be operatively coupled to a noble gas source to feed noble gas to said inner noble gas conduit such that said electrode at least partially ionizes the noble gas to generate the plasma stream to be directed to the surgical site to perform the surgical procedure; and

an outer aspiration conduit including a distal end and a proximal end disposed in surrounding coaxial relation relative to said inner noble gas conduit to cooperatively form an aspiration channel therebetween, said outer aspiration conduit configured to be operatively coupled to a negative pressure source, said distal end of said outer aspiration conduit extending beyond said distal end of said inner noble gas conduit to remove fluid and solid debris from the surgical site.

6. The electrosurgical handpiece of claim 5, further an intermediate electronegative gas conduit disposed in surrounding relation relative to said noble gas conduit to cooperatively form an electronegative gas channel therebetween

coupled to a gas source to feed electronegative gas to said electronegative gas channel such that said electronegative gas sustains said plasma stream.

7. The electrosurgical handpiece of claim 6, wherein said intermediate electronegative gas conduit is further configured to be coupled to a saline solution source for intermittently substituting a saline solution for the electronegative gas to enhance debris removal.

8. The electrosurgical handpiece of claim 6, wherein said intermediate gas conduit is coupled to a second noble gas source to feed noble gas to the electronegative gas channel to form a secondary plasma stream to at least partially envelop said plasma stream to at least partially ionize the secondary plasma stream.

9. An electrosurgical generator for use with an electrosurgical device to generate a plasma stream for performing electrosurgery on a surgical site on a patient coupled to an electrical power source to supply power to the electrosurgical device, the electrosurgical generator comprises a transformer coupled to the electrical power source to provide high frequency electrical energy to the plasma generator, the transformer comprising a step-down stage including a primary and secondary and a step-up stage including a primary and secondary operatively coupled together,

the primary of the step-down stage being coupled to the electrical power source, the secondary of the step-down stage being coupled to the primary of the step-up stage and the secondary of the step-up stage being coupled to an electrode of the electrosurgical device,

wherein the transformer provides a substantially constant potential.

10. The electrosurgical generator of claim 9, wherein the secondary of the step-up stage is coupled between the electrode through a conductor and an isolated nonfloating return path.

11. The electrosurgical generator of claim 10, wherein the step-up stage further includes a capacitor in series with the electrode to supply a substantially constant output current to the surgical site.

12. The electrosurgical generator of claim 10, wherein the primary of the step-down stage is coupled across a power amplifier.

13. The electrosurgical generator of claim 9, wherein the electrosurgical generator comprises an isolated nonfloating potential.

14. The electrosurgical generator of claim 13, wherein the electrosurgical generator includes a return current circuit comprising the tissue and body fluid and the patient, and the combined external capacitance of the operator and displacement current in the air.

15. The electrosurgical generator of claim 9, wherein the electrosurgical generator includes a return current circuit comprising the tissue and body fluid and the patient, and the combined external capacitance of the operator and displacement current in the air.

16. The electrosurgical generator of claim 15, wherein the electrosurgical generator comprises an isolated nonfloating potential.

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专利名称(译)	电外科设备产生等离子流		
公开(公告)号	US20120065635A1	公开(公告)日	2012-03-15
申请号	US13/295261	申请日	2011-11-14
[标]申请(专利权)人(译)	博维医药公司		
申请(专利权)人(译)	bovie刀医疗法人		
当前申请(专利权)人(译)	bovie刀医疗法人		
[标]发明人	KONESKY GREGORY A		
发明人	KONESKY, GREGORY A.		
IPC分类号	A61B18/14 A61B18/00		
CPC分类号	A61B2218/008 A61B18/042		
其他公开文献	US8409190		
外部链接	Espacenet USPTO		

摘要(译)

一种用于产生等离子体流的电外科装置和在患者体内进行内窥镜或腹腔镜手术的方法。电外科装置包括可操作地连接到电外科发生器以从其接收电能的电极，电极同心地设置在内部惰性气体导管内以形成等离子体通道。外部电负性气体导管以相对于内部惰性气体导管的周围同轴关系设置，以在它们之间协作地形成电负性气体通道，使得电极加热惰性气体以至少部分地电离惰性气体以产生待引导的等离子体流。在电负性气体维持手术部位处的血浆流并且稀释手术部位附近的惰性气体时，到手术部位进行外科手术。可以提供外部抽吸导管以从手术部位移除流体和固体碎屑。

