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Mantell et al.(10) **Pub. No.: US 2002/0183715 A1**(43) **Pub. Date: Dec. 5, 2002**(54) **LAPAROSCOPIC INSERTION DEVICE****Publication Classification**(76) Inventors: **Robert R. Mantell**, Arlington Heights,
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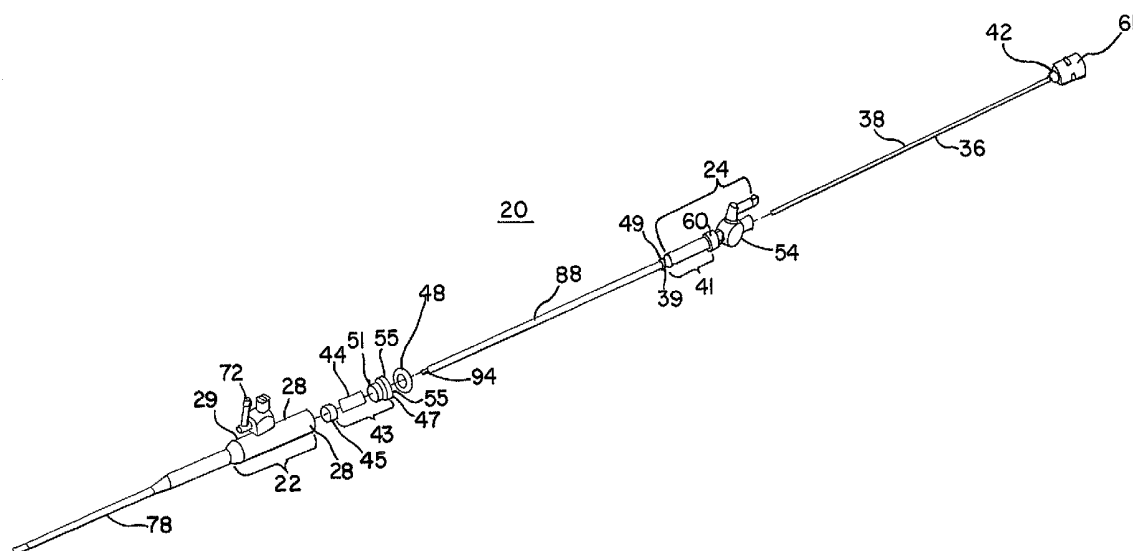
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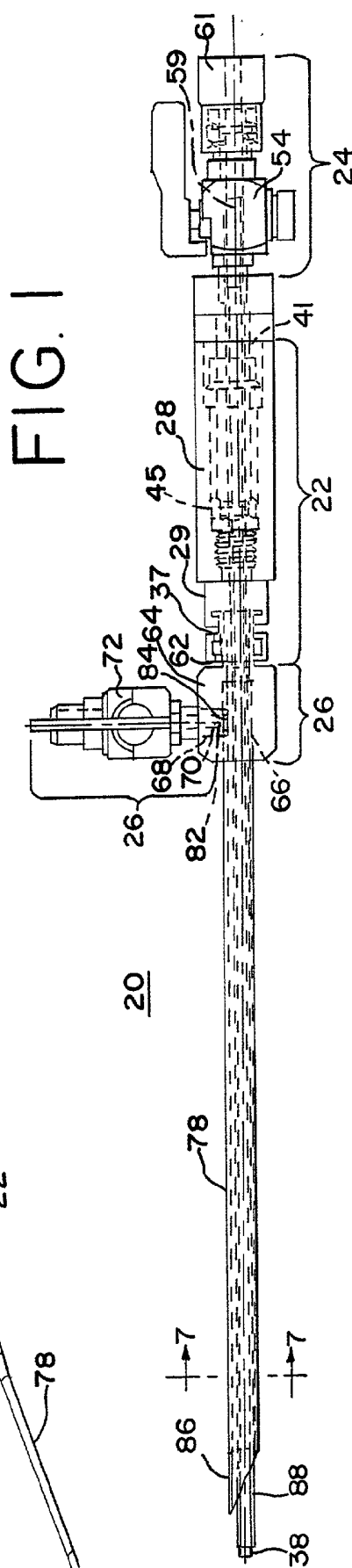
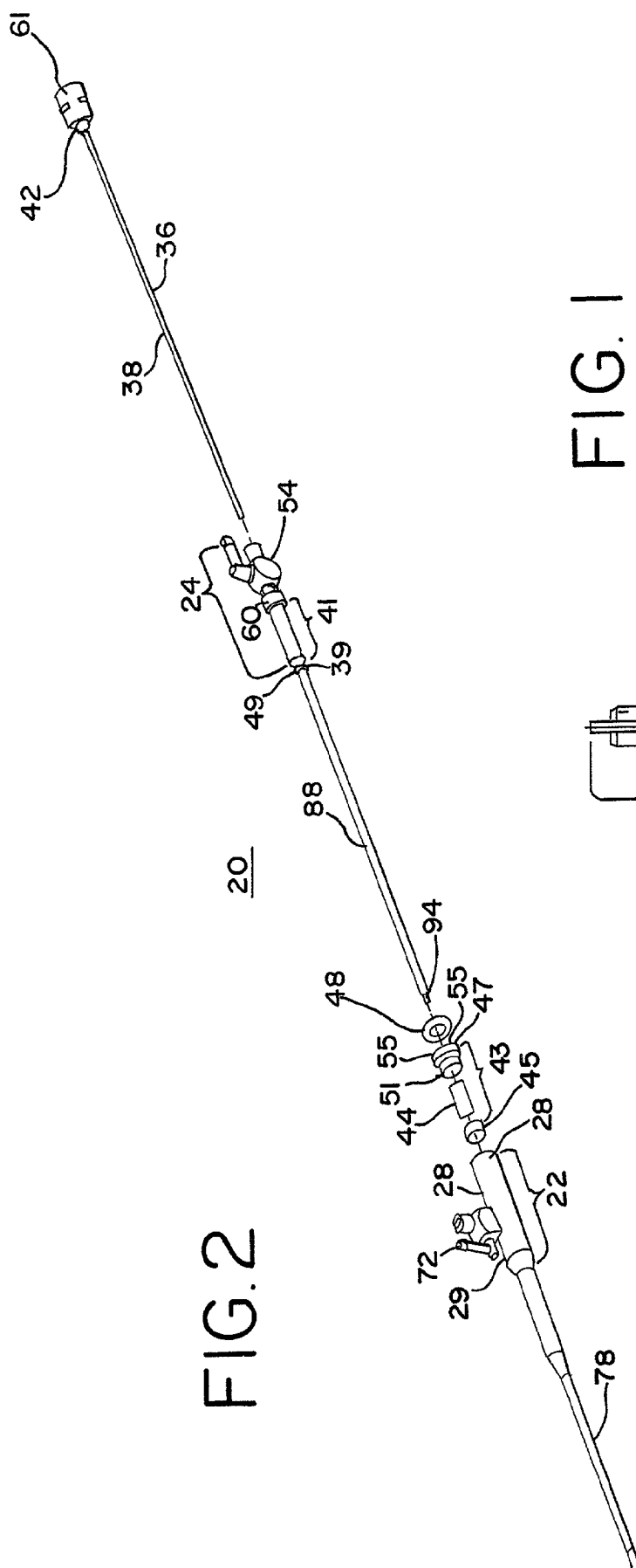
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ABSTRACT

A method of treatment of a body cavity of an animal that includes inserting a portion of an insertion device into a body cavity of an animal and simultaneously supplying from the inserted insertion device a first fluid and either a medical instrument or a second fluid into the body cavity, wherein the first fluid and either the medical instrument or the second fluid are not in fluid communication with one another within the insertion device.

(21) Appl. No.: **09/841,125**(22) Filed: **Apr. 24, 2001**



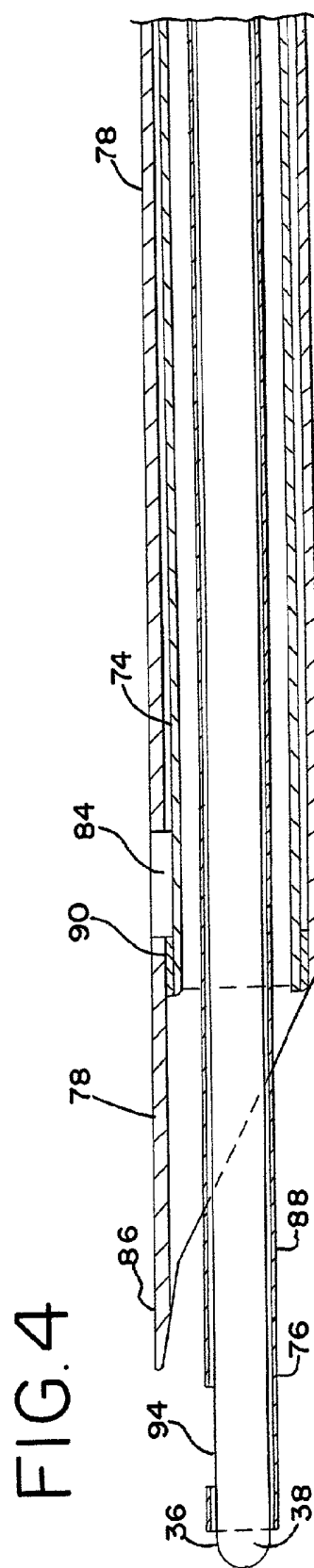
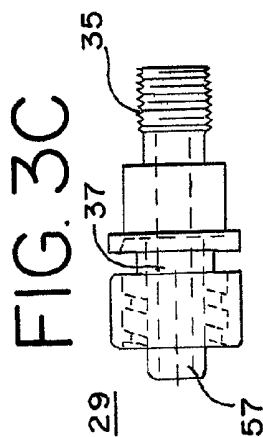
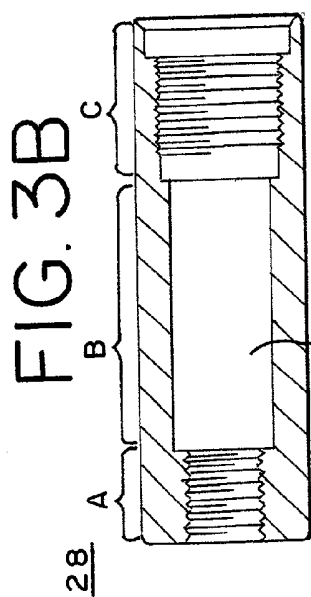
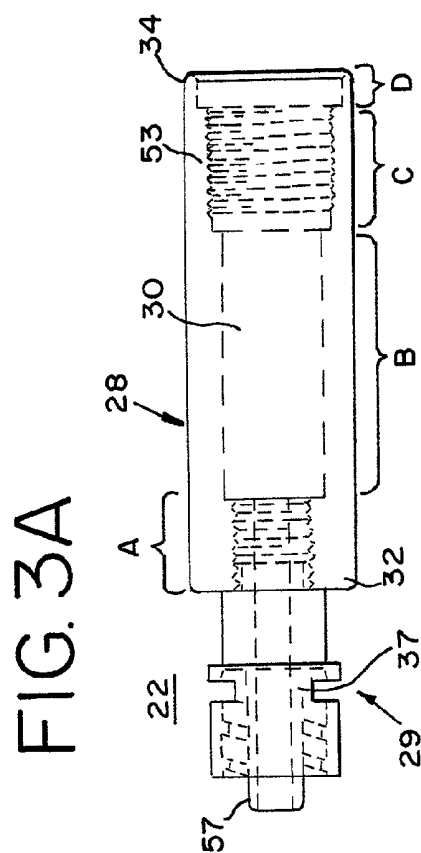


FIG. 5

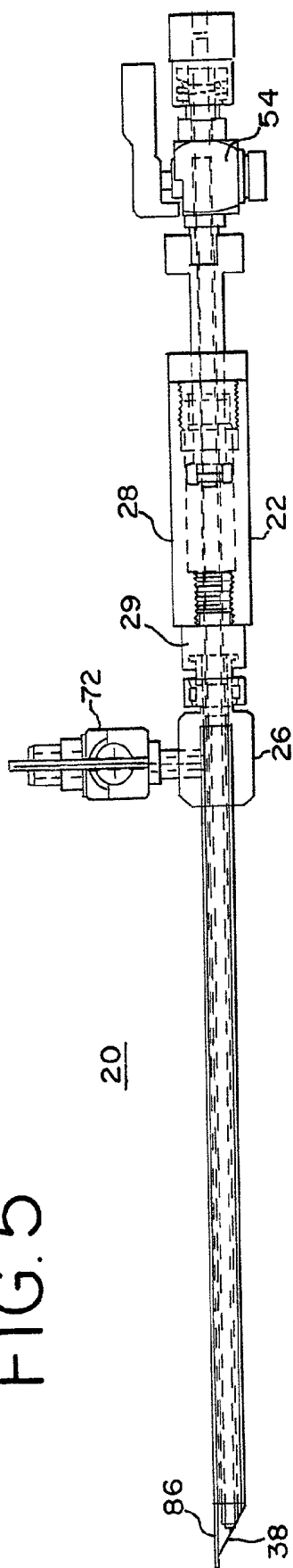
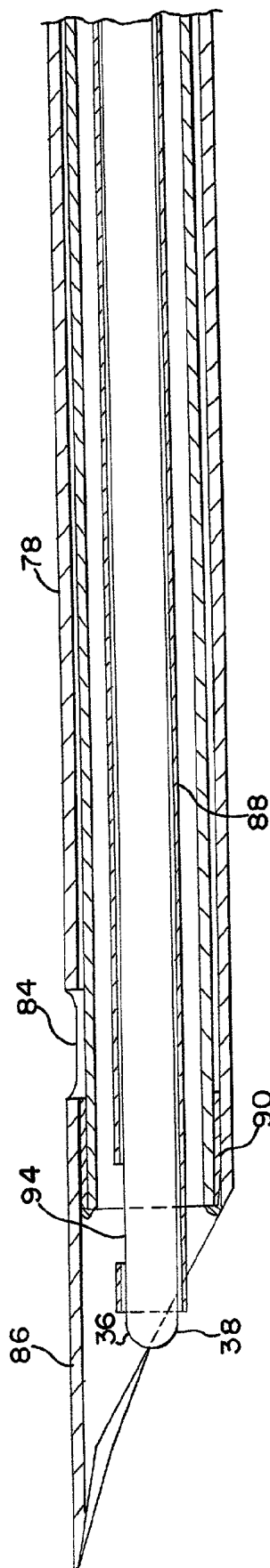
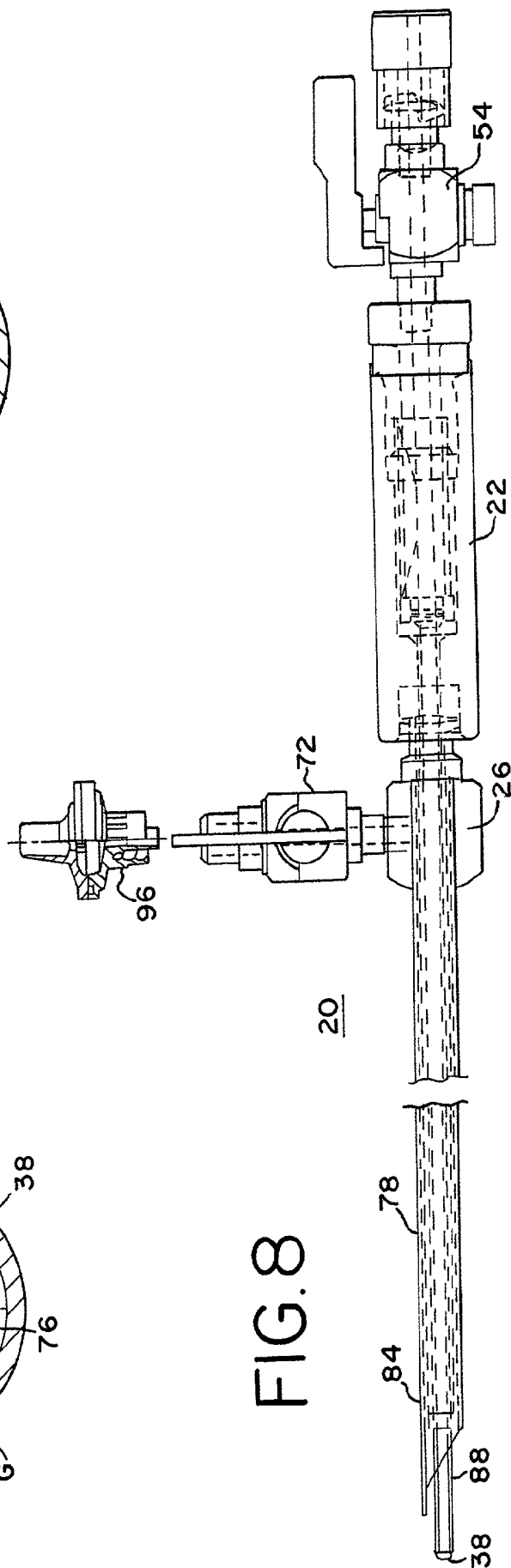
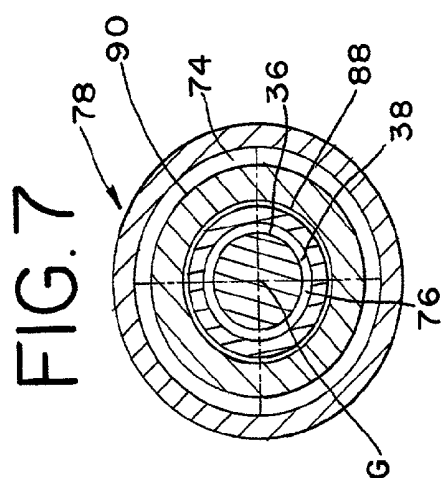
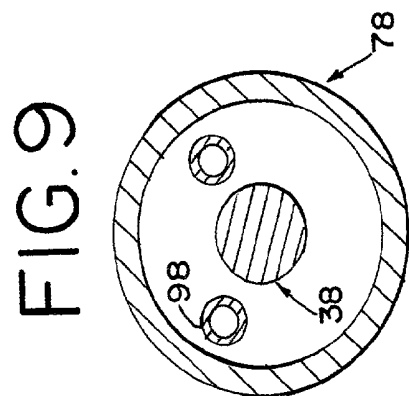


FIG. 6





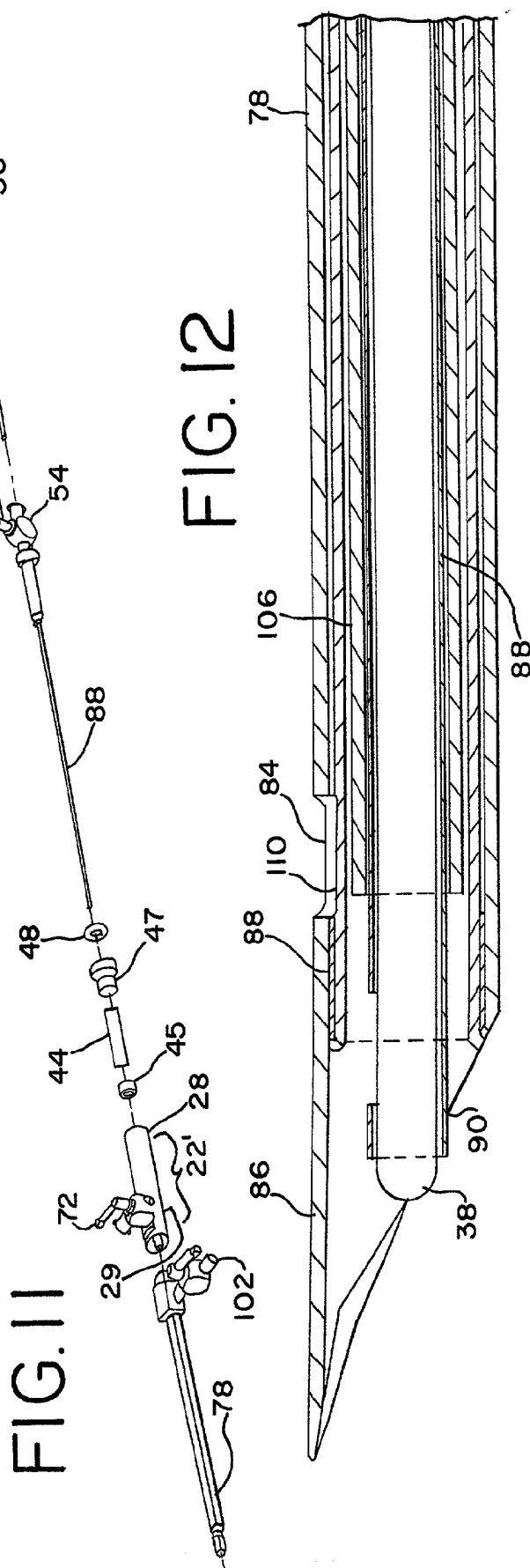
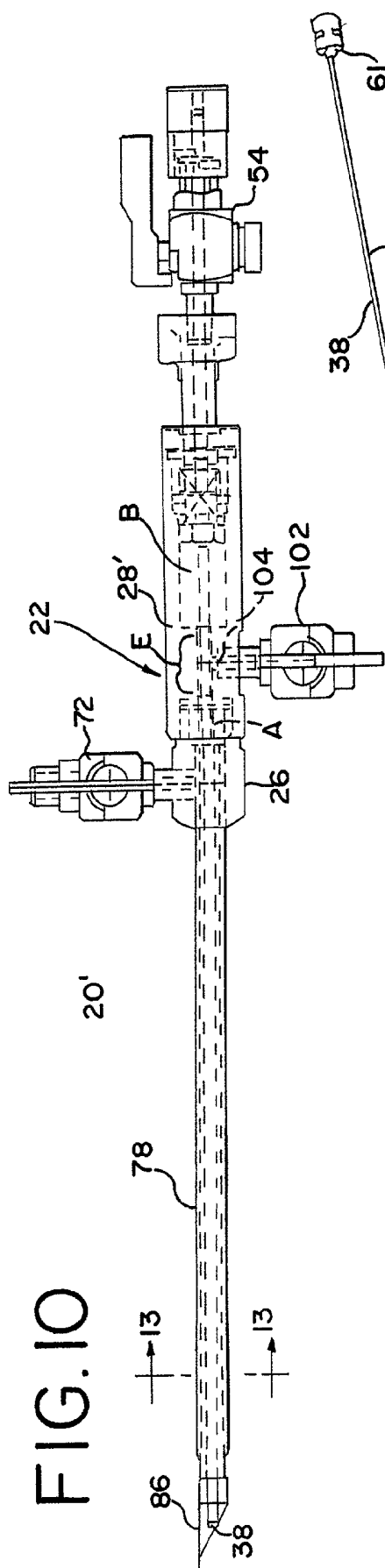


FIG. 15

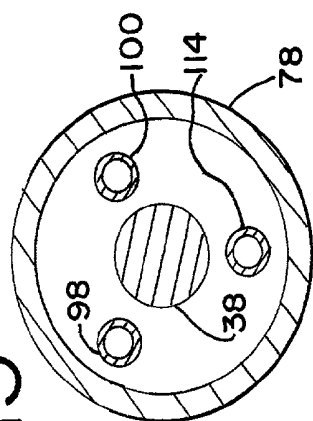


FIG. 13

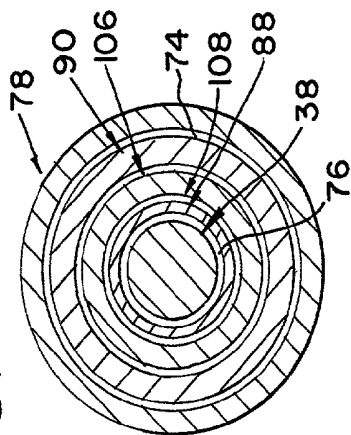
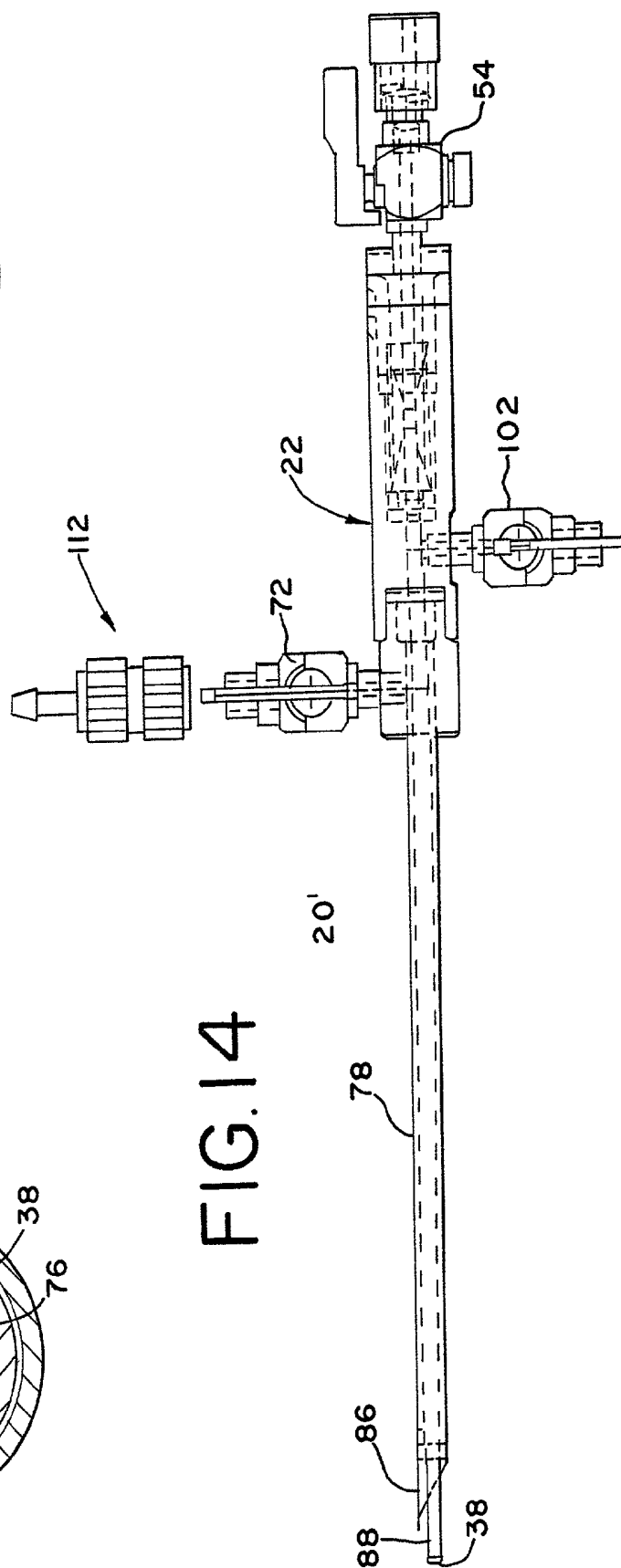
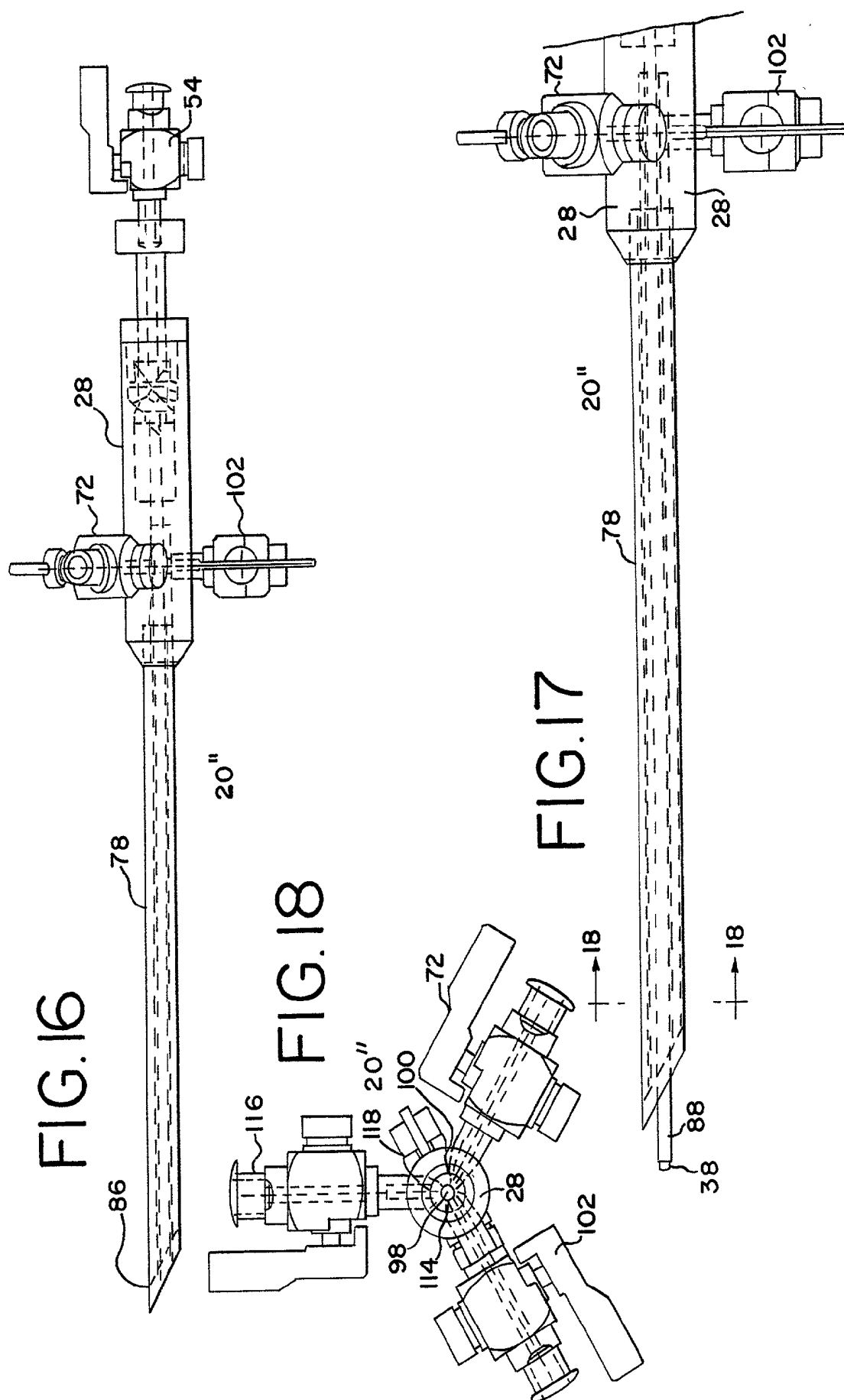


FIG. 14





LAPAROSCOPIC INSERTION DEVICE

BACKGROUND OF THE INVENTION

[0001] 1. Field of the Invention

[0002] The present invention relates generally to instruments for laparoscopic surgery. In particular, it relates to an improved laparoscopic surgical instrument that can simultaneously perform multiple tasks and procedures independent of one another.

[0003] 2. Discussion of Related Art

[0004] Laparoscopic surgery involves the use of small incisions to insert surgical instruments of 3-10 millimeter (mm) diameter into the abdominal cavity. In performing such surgery, telescopes of 5-11 mm diameter usually also are inserted through the abdominal wall in order to view intraabdominal contents during the surgery. The initial step in laparoscopic surgery is to insert a needle of about 2 mm diameter through the abdominal wall such that the tip of the needle lies in the abdominal cavity itself. About 2-4 liters of a medical grade sterilized gas such as carbon dioxide, is insufflated through the needle and into the cavity. This procedure separates the abdominal wall from the organs and also usually separates the organs from one another, as the case may be.

[0005] The traditional device for passage of an insufflating gas is the Verres needle which comprises an outer cannula which has a distal needle-like tip for puncturing the abdominal wall and an expanded opposite portion which houses a spring mechanism for retraction of an inner cannula or obturator.

[0006] The obturator comprises a hollow tube having an enclosed, rounded distal end with a lateral port in close proximity to the said distal end. As the Verres needle penetrates the epidermis and abdominal wall, the obturator retracts into the outer cannula against the bias of the spring to facilitate penetration through the abdominal wall. After penetration of the abdominal wall, the distal end of the obturator is spring-biased out of the Verres needle into the abdominal cavity. An insufflating gas then is delivered to the abdominal cavity from a gas supply detachably connected to the Verres needle so that the insufflating gas can enter the expanded portion of the outer cannula and traverse inside the inner cannula and enter the abdominal cavity through the lateral port located in the distal end of the inner cannula. In this case, the obturator and insufflating gas share a common passage or channel within the inner cannula. The insufflating gas serves to separate the abdominal wall from underlying organs.

[0007] In some known devices, the obturator can be removed so that a medical instrument, such as an endoscope, can be inserted into the space vacated by the obturator and inserted into the abdominal cavity. One disadvantage of the inserting the medical instrument into the Verres needle is that the medical instrument causes a significant restriction to the flow of insulating gas within the Verres needle since the medical instrument and the insufflating gas share a common passage or channel in the inner cannula. Such restriction in flow of the insufflating gas can limit the effectiveness of the insufflator.

[0008] Known trocars are similar to the above-described Verres needle in that they have a cannula that forms a single

passage that contains both the insufflating gas and an obturator. One difference between a trocar and a Verres needle is that the Verres needle is typically a 14 gage needle size while trocars are known to have sizes ranging from 10 to 12 mm. One similarity between a trocar and a Verres needle is that the trocars are known that allow the obturator to be removed so that a medical device, such as an endoscope, can be inserted into the cannula. Like the Verres needle described previously, inserting the medical instrument into the cannula causes a significant restriction to the flow of insufflating gas within the trocar due to the sharing of a common passage by the medical instrument and the insufflating gas.

[0009] Another disadvantage of insertion devices, such as Verres needles and trocars, is that only one fluid can be conveyed within the insertion device at any one time. If multiple fluids are needed to be conveyed to or from the abdominal cavity for instance, then multiple Verres needles or trocars would be needed where each Verres needle or trocar is associated with only one of the multiple fluids. Using multiple insertion devices lead to the disadvantages of increasing the cost of the procedure, the complexity of the procedure and potentially increasing trauma incurred by the patient.

[0010] In the alternative, a single Verres needle or trocar could be used where one of the multiple fluids would be conveyed at one period of time and the other multiple fluids would be conveyed at separate and distinct time. Such a mode of operation could lead to contamination of the Verres needle or trocar with multiple fluids, increase the complexity of timing the application of fluids and requiring special metering and/or control devices.

SUMMARY OF THE INVENTION

[0011] One aspect of the present invention regards an insertion device that includes a housing, a first port attached to the housing for receiving a first fluid and a first chamber connected to the first port and positioned within the housing, wherein the first chamber has an opening that is in fluid communication with a target area. A second port attached to the housing for receiving a second fluid and a second chamber connected to the second port and positioned within the housing, wherein the second chamber has an opening that is in fluid communication with the target area, wherein the first chamber and the second chamber are permanently not in fluid communication with one another and simultaneously are in fluid communication with the target area.

[0012] A second aspect of the present invention regards a method of treatment of a body cavity of an animal that includes inserting a portion of an insertion device into a body cavity of an animal and simultaneously supplying from the inserted insertion device a first fluid and a second fluid into the body cavity, wherein the first fluid and the second fluid are not in fluid communication with one another within the insertion device.

[0013] A third aspect of the present invention regards a method of treatment of a body cavity of an animal that includes inserting a portion of an insertion device into a body cavity of an animal and simultaneously supplying from the inserted insertion device a fluid and a medical instrument into the body cavity, wherein the first fluid and the medical instrument are not in fluid communication with one another within the insertion device.

[0014] Each aspect of the present invention provides the advantage of improving fluid flow in an insertion device during a laparoscopic procedure.

[0015] Each of the first two aspects of the present invention provides the advantage of decreasing the cost of laparoscopic procedures by using a single insertion device for simultaneously conveying multiple fluids during a laparoscopic procedure.

[0016] Each of the first two aspects of the present invention provides the advantage of decreasing the complexity of laparoscopic procedures by simultaneously conveying multiple fluids during a laparoscopic procedure.

[0017] Each of the first two aspects of the present invention provides the advantage of reducing the risk of contamination of an insertion device by multiple fluids conveyed by the insertion device during a laparoscopic procedure.

[0018] The present invention, together with attendant objects and advantages, will be best understood with reference to the detailed description below in connection with the attached drawings.

BRIEF DESCRIPTION OF THE DRAWINGS

[0019] FIG. 1 is a side, partially transparent view of an embodiment of an insertion device in an extended mode according to the present invention;

[0020] FIG. 2 is a perspective, partially exploded view of the insertion device of FIG. 1;

[0021] FIG. 3A is a side cross-sectional view of an embodiment of a lumen sub-assembly to be used with the insertion device of FIG. 1;

[0022] FIG. 3B is a side cross-sectional view of an embodiment of a lumen housing to be used with the lumen sub-assembly of FIG. 3A;

[0023] FIG. 3C is a side cross-sectional view of an embodiment of a lumen housing adapter to be used with the lumen sub-assembly of FIG. 3A;

[0024] FIG. 4 is an enlarged side, partially transparent view of an end of the insertion device of FIG. 1 in an extended mode;

[0025] FIG. 5 is a side, partially transparent view of the insertion device of FIG. 1 in a retracted mode;

[0026] FIG. 6 is an enlarged side, partially transparent view of an end of the insertion device of FIG. 1 in a retracted mode;

[0027] FIG. 7 is cross-sectional view of the insertion device of FIG. 1 as taken along lines 7-7 of FIG. 1;

[0028] FIG. 8 is a side, partially transparent view of a second embodiment of an insertion device in an extended mode according to the present invention;

[0029] FIG. 9 is a cross-sectional view of a third embodiment of an insertion device according to the present invention;

[0030] FIG. 10 is a side, partially transparent view of a fourth embodiment of an insertion device in a retracted mode according to the present invention;

[0031] FIG. 11 is a perspective, partially exploded view of the insertion device of FIG. 10;

[0032] FIG. 12 is an enlarged side, partially transparent view of an end of the insertion device of FIG. 10 in a retracted mode;

[0033] FIG. 13 is a cross-sectional view of the insertion device of FIG. 10 as taken along lines 13-13 of FIG. 10;

[0034] FIG. 14 is a side, partially transparent view of a fifth embodiment of an insertion device in an extended mode according to the present invention;

[0035] FIG. 15 is a cross-sectional view of a sixth embodiment of an insertion device according to the present invention;

[0036] FIG. 16 is a side, partially transparent view of a seventh embodiment of an insertion device in a retracted mode according to the present invention;

[0037] FIG. 17 is an enlarged side, partially transparent view of the insertion device of FIG. 16 in an extended mode; and

[0038] FIG. 18 is cross-sectional view of the insertion device of FIG. 16 taken along lines 18-18 of FIG. 17.

DETAILED DESCRIPTION OF THE INVENTION

[0039] Referring now to FIGS. 1-7, an insertion device, such as Verres needle 20, includes a lumen housing sub-assembly 22, a first fluid port section 24 and a second fluid port section 26.

[0040] As shown in FIGS. 1, 2, 3A-B and 5, the lumen housing sub-assembly 22 includes a cylindrical-like lumen housing 28 that is threadedly attached to a lumen housing adapter 29. As shown in FIGS. 3A-B, the lumen housing 28 includes a central channel 30 that extends from a distal end 32 to a proximal end 34 of the lumen housing 28. The central channel 30 has a length of approximately 1.437 inches. The channel 30 has a diameter that varies in a step-like manner. For example, the channel 30 has four distinct portions: 1) a distal portion A that has a diameter of approximately 0.36 inches and a length of approximately 0.312 inches, 2) an intermediate distal portion B that has a diameter of approximately 0.302 inches and a length of approximately 0.725 inches, an intermediate proximate portion C that has a diameter of approximately 0.302 inches and a length of approximately 0.40 inches, and a proximal portion D that has a diameter of approximately 0.5 inches and a length of approximately 0.158 inches.

[0041] The portion A of the central channel 30 is threaded, receives and is attached to a threaded male member 35 of a lumen housing adapter 29 as shown in FIG. 3A. The lumen housing adapter 29 has an opening 37 that is aligned with the channel 30 of the lumen housing 28. The attached lumen housing adapter 29 and lumen housing 28 constitute the lumen housing sub assembly 22. Note that a distal end 57 of the lumen housing adapter 29 is attached via silver solder to a needle cannula exterior housing 78. As shown in FIGS. 1, 2 and 4-7, the housing 78 is substantially cylindrical/annular in shape having a length of approximately 4.970 inches, an inner diameter of approximately 0.173 inches and an outer diameter of approximately 0.203 inches. The housing 78 has

a 0.093 inch diameter opening **80** that is aligned with an opening **82** of the fluid port section **26**. The opening **80** is approximately 0.24 inches from a proximal end of the housing **78**. The housing **78** has a second opening **84** formed approximately 4.09 inches from the opening **80** and further includes a needle **86** formed at a distal end thereof. The housing **78** is preferably made of stainless steel.

[0042] As shown in FIGS. 1, 2 and 5, the portions A-D of the central channel **30** and the opening **37** receive an inner needle cannula wall **88** that is inserted into and welded into an opening **39** of a cylindrical-like extension **41** of a port, such as stopcock **54**, that forms part of the fluid port section **24**. The inner needle cannula wall **88** is annular/cylindrical in shape having a length of approximately 7.282 inches, an inner diameter of approximately 0.84 inches and an outer diameter of approximately 0.93 inches. As shown in FIGS. 1, 2 and 4-6, the inner needle cannula wall **88** is inserted into the interior of the housing **78** and has a distal end that is near the distal end of the housing **78**.

[0043] As shown in FIG. 2, the inner needle cannula wall **88** is also inserted into an O-ring seal **48** and a bias mechanism **43** that includes a spring **44**, a stop **45** and a compression piece **47**. In particular, the inner needle cannula wall **88** is inserted into aligned openings of the O-ring seal **48**, the compression piece **47**, the spring **44** and the stop **45**. Once the inner needle cannula wall **88** is inserted, the stop **45** is threaded onto a threaded end portion **49** of the extension **41** of the fluid port section **24**. At this stage, the extension **41** passes through the aligned openings of the spring **44**, compression piece **47** and O-ring seal **48**. The extension **41** is inserted into channel **30** of the lumen housing **28** and the compression piece **47** is inserted into portion C of channel **30** of the lumen housing **28**. The exterior threads **51** of the compression piece **47** threadedly engage the threads **53** of portion C of channel **30**. The end result of the threaded attachment of stop **45** and compression piece **47** is that the spring **44** is captured between the stop **45** and compression piece **47**. In addition, the lumen housing **28** is able to slidingly move relative to the fluid port section **24** along the longitudinal length of the extension **41**. Such movement is limited in that the compression piece **47** attached to the lumen housing **28** is constrained to move from where the stop **45** is attached to extension **41** to where the O-ring seal **48** that is welded to an annular shoulder **60** of the extension **41**. The O-ring seal **48** seals the space between lumen housing **28** and extension **41** when a proximal end **55** of the compression piece **47** abuts against the O-ring seal **48**.

[0044] After the lumen housing **28** is attached to the fluid port section **24** via bias mechanism **43**, an annular-like stainless steel wall **36** of an obturator **38** is inserted into a longitudinal channel **59** formed in the fluid port section **24**. The obturator **38** has a length of approximately 8.75 inches and a diameter of approximately 0.063 inches. As shown in FIG. 2, the obturator **38** has a rounded distal end **40**. As shown in FIGS. 1, 2 and 5, the proximal end **42** of the obturator **38** is attached via silver solder to a cap **61**. The cap **61** has threads that engage a proximal end of the stopcock **54**. The cap **61** prevents the obturator **38** from exiting the distal end of the housing **78**. As shown in FIGS. 1, 2 and 4-6, the obturator **38** is inserted into the interior of the inner needle cannula wall **88** and has a distal end that is near the distal end of the housing **78**.

[0045] With the obturator **38** positioned within the inner needle cannula wall **88** and the housing **78**, the Verres needle **20** allows for both the obturator **38** and the inner needle cannula wall **88** to be movable relative to the housing **78** from an extended position to a retracted position and vice versa. In the case of the extended position, when no forces are pushing the inner cannula wall **88** toward the proximal end of the Verres needle **20**, the spring **44** is maintained at its natural length and so the distal end of the inner cannula wall **88** extends past the housing **78** as shown in FIGS. 1 and 4. Thus, the spring **44** normally biases the inner needle cannula wall **88** to an extended position shown in FIGS. 1 and 4. When no forces are pushing the obturator toward the proximal end of the Verres needle **20**, the obturator **38** also extends past the housing **78** as shown in FIGS. 1 and 4. Note that when the inner needle cannula wall **88** is at the extended position, the proximal end **55** of the compression piece **47** seals the O-ring **48** between itself and the shoulder **60**. The retracted position is achieved when a force pushes the inner cannula wall **88** toward the proximal end of the Verres needle **20**. Such pushing causes the distal end of the inner cannula wall **88** to enter into the housing **78** and causes the stop **45** and the distal end of the spring **44** to move toward the proximal end of the Verres needle **20** as shown in FIG. 5. This causes the spring **44** to be compressed. When a force pushes the obturator toward the proximal end of the Verres needle **20**, the distal end of the obturator **38** also enters into the housing **78** as shown in FIGS. 5 and 6.

[0046] As shown in FIGS. 1 and 3, the second fluid port section **26** has a threaded male member **62** that engages threads **63** formed in the distal portion **57** of the lumen housing adapter **29**. The threaded male member **62** is integrally attached to a body **64** that includes an axially extending channel **66** and a radially extending channel **68**.

[0047] The radially extending channel **68** is threaded and is in fluid communication with the axially extending channel **66**. As shown in FIGS. 1 and 5, a threaded male member **70** of a port, such as stopcock **72**, is inserted into and threadedly engages the channel **68**.

[0048] The stopcocks **54** and **72** preferably are attached to supplies (not shown) for two isolated fluids. Thus, the stopcocks **54** and **72** allow for two different fluids, to be supplied to the Verres needle **20**. For example, stopcocks **54** and **72** can be attached to separate supplies of carbon dioxide. In another embodiment, one of the stopcocks **54** can be attached to a supply of carbon dioxide while the other stopcock is attached to a supply of an aerosolized medication. In accordance with the present invention, the two fluids are permanently not in fluid communication with one another. Note that in this application, the term fluid is deemed to include either a gas or a liquid.

[0049] Isolation between the two fluids is accomplished by a pair of chambers **74** and **76** that are formed within the needle cannula exterior housing **78**. The annular chamber **74** is defined as the space between the housing **78** and a cannula wall **90**. The cannula wall **90** is annular/cylindrical in shape having a length of approximately 4.562 inches, an inner diameter of approximately 0.134 inches and an outer diameter of approximately 0.165 inches. The cannula wall **90** is attached to housing **78** by silver solder. In particular, silver solder is applied to the housing **78** and wall **90** distally of the opening **84**. Silver solder is also applied to the housing **78**

and wall 90 proximally of opening 82. The silver solder seals the chamber 74 at distal and proximal ends thereof. As shown in FIG. 7, the housing 78 and the wall 90 are concentric about a common axis G so that the annular chamber 74 is concentric about axis G as well. The housing 78 and the wall 90 are spaced from one another by approximately 0.080 inches.

[0050] In operation, the stopcock 72 is opened so that a fluid is received by the opening 82 and delivered into the opening 80 of the housing 78. The fluid then flows into the chamber 74 and exits out of the opening 84 of the housing and the annular space 74 between housing 78 and wall 90 and flows into a target area, such as a body cavity or abdomen. Thus, the opening 84 is in fluid communication with a target area.

[0051] A second annular chamber 76 is defined as the space between an annular portion of the wall 36 of the obturator 38 and an inner needle cannula wall 88. As shown in FIG. 5, the wall 36 and the cannula wall 88 are concentric about axis G so that the annular chamber 76 is concentric about axis G as well. The wall 36 and the cannula wall 88 are spaced from one another by approximately 0.021 inches. In addition, the wall 88 is movable relative to the housing 78 in that it is attached to the extension 41 of the stopcock 54, which is biased via spring 44 so as to move relative to the housing 78. As mentioned previously, the obturator 38 and wall 36 are attached to the stopcock 54 as well via cap 51. Thus, when stopcock 54 and wall 88 move relative to housing 78, the obturator 38 and wall 36 will also move with stopcock 54 and so move in unison with the wall 88.

[0052] As shown in FIGS. 1 and 4-6, the obturator 38, the cannula wall 88 and the annular chamber 76 extend from the distal end of the Verres needle 20 to a distal opening 39 formed in the stopcock 54. In operation after the Verres needle 20 is inserted into the body cavity or abdomen and the obturator 38 is removed after the cap 61 is unthreaded and attached from the stopcock 54, the stopcock 54 remains open so that a fluid is received by the opening 59 and delivered into the annular chamber 76. The fluid then flows the entire length of the chamber 76 and exits a distal opening 94 and the distal end of the chamber 76 and flows into a target area, such as a body cavity or abdomen. Thus, the opening 94 and the distal end of the chamber 76 are in fluid communication with a target area.

[0053] When both stopcock 54 and 72 are open at the same time, the fluids associated with the stopcocks flow within the Verres needle 20 do not intermingle within the needle 20 since the annular walls 78 and 90 do not define a volume of space that is common with any volume of space defined by the annular walls 36 and 88. Accordingly, the chambers 74 and 76 are isolated from one another so they are permanently not in fluid communication with one another. The fluids are then expelled out of the Verres needle 20 into the target area so that the chambers 74 and 76 simultaneously are in fluid communication with the target area.

[0054] The Verres needle 20 described above with respect to FIGS. 1-7 can be used in a variety of medical procedures to be performed on an animal, such as a human being. In a typical method of treatment, the needle 86 of the housing 78 is used pierce an area of a human patient. During the piercing, the obturator 38 and the cannula wall 88 are pushed by the patient's tissue to a retracted position as shown in

FIGS. 5 and 6. Such pushing causes spring 44 to compress as well. Once the needle 86 enters a target area, such as the chest cavity or the abdomen of the human patient, the pressure exerted by the tissue is absent causing spring 44 to expand which results in cannula wall 88 to move to the extended position shown in FIGS. 1 and 4. Since the obturator 38 is mechanically joined to the cannula wall 88, the obturator 38 also moves to the extended position once the needle 86 enters the target area. Upon noticing that the obturator 38 has moved to the extended position, the surgeon determines that the Verres needle 20 has entered into the abdomen whereupon the cap 61 is unthreaded from the stopcock 54, the obturator 38 is removed and an insufflation gas is then directed into the abdomen by opening up either stopcock 54 or 72. With the obturator 38 retained or removed, fluids can be delivered or received within space 74 by utilizing stopcock 72.

[0055] The insufflation gas expands the abdomen so that laparoscopic procedures and monitoring can be performed. For example, while the insufflation gas is supplied to the chest cavity or abdomen via chamber 74, for example, the other chamber 76 can be used to simultaneously perform a continuous pressure measurement of the peritoneum. This allows for faster insufflation because the pressure would be read continuously and the insufflator would flow gas continuously to the body cavity via chamber 74 instead of in a stop and start mode that is currently used.

[0056] In another mode of operation during insufflation via chamber 74, the other chamber 76 can be adapted to receive a medical instrument by the open stopcock 54 and removing the obturator 38 when access to that space is required. Possible medical instruments that can be fed into chamber 76 into the abdomen are: 1) fluid pumps, such as hand pumps, syringe pumps, peristaltic pumps, centrifugal pumps, etc., 2) wall suction, or portable vacuum suction pumps, 3) graspers, scissors, electro-surgical tools, suction/irrigation wands, regular or mini endoscopes, etc., 4) catheters (such as aerosolization ala TMI), 5) infusion devices (gravity fluid bags), syringe injection, biopsy needles etc., 6) humidification devices (evaporative media), and 7) filtering devices, passive (filter media) or active (withdraw a fluid, filter it, and replace it). An example of using a filtering device is shown in FIG. 8 where a filter 96 is attached to stopcock 72 in a well known manner.

[0057] Besides the medical instruments mentioned above that treat the abdomen, monitoring devices can be connected to the chamber 76, such as 1) pressure relief valves, passive (mechanical) or controlled (electronic) pressure transducers, 2) thermocouples, RTD's, thermistors, etc (temperature), 3) CCD cameras, chip (solid state) cameras, and 4) ultrasonic, and humidity measuring devices.

[0058] Note that depending on the particular instrument or monitoring involved mentioned above, the stopcock 54 of chamber 76 can be replaced by or used in conjunction with well known rubber seals, injection ports, flap valves and iris valves.

[0059] There are many ways in which the Verres needle 20 of FIGS. 1-7 can be used. The matrix set forth below shows some of the many possibilities in which the Verres needle 20 conducts a number different functions and or use of devices to enhance medical techniques. Note that the columns of the matrix indicate possible applications that can be performed

by one of the ports **54**, **72** while the rows indicate applications that can be performed by the other port. An X indicates that the applications for the corresponding row and column can be performed simultaneously. Although the matrix would indicate that only two of the categories would be used in conjunction with each other, in reality, as many of these could be used in combination as is practical to design the introducer (three, four, or five, etc) if the operative area would allow for one device to be used.

| | Infus- ing gas | Infus- ing liquid | Suction- ing Gas | Suction- ing liquid | Venting or pressure relief | Tool entry (instru- ment) | Catheter entry |
|----------------------------------|----------------------|-------------------------|------------------------|---------------------------|-------------------------------------|------------------------------------|-------------------|
| Infusing gas | — | X | X | X | X | X | X |
| Infusing liquid | X | — | X | X | X | X | X |
| Suctioning gas | X | X | — | X | X | X | X |
| Suctioning liquid | X | X | X | — | X | X | X |
| Venting or pressure relief | X | X | X | X | — | X | X |
| Tool entry (instru- ment) | X | X | X | X | X | — | X |
| Catheter entry | X | X | X | X | X | X | — |
| Measure pressure | X | X | X | X | X | X | X |
| Measure Tempera- ture | X | X | X | X | X | X | X |
| Measure Flow | X | X | X | X | X | X | X |
| Endo- scopic port | X | X | X | X | X | X | X |
| Camera (chip) port | X | X | X | X | X | X | X |
| Medica- tion infusion | X | X | X | X | X | X | X |
| Moisture infusion | X | X | X | X | X | X | X |

[0060] In summary, the isolated chambers **74** and **76** allow for multiple fluids to be conveyed to a target area. The isolated chambers **74** and **76** allow for a fluid to be supplied to the target area via one chamber while the other chamber simultaneously receives a fluid from the target area. The isolated chambers **74** and **76** also allow for simultaneous supply to or removal of a fluid from a target area while a medical instrument is supplied to the target area via the other chamber. The isolated chambers **74** and **76** allow for simultaneous use of medical instruments and/or monitor devices in the target area. Note that when a medical instrument or monitor device is to be inserted into chamber **76**, the obturator **38** can be removed in a well known manner so as to increase the volume of the chamber **76**.

[0061] While the above description regards using isolated chambers **74** and **76** that are annular and concentric, it is possible to replace the annular walls **88** and **90** of FIGS. 1-8 with separate and nonintersecting tubes **98** and **100** that are shown in FIG. 9. The tube **98** extends from the opening **92** to the distal end of the housing **78**. Similarly, tube **100**

extends from the opening **80** to the distal end of the housing **78**. The tubes **98** and **100** are preferably made of stainless steel or plastic and have a diameter of approximately 0.160 inches. When made of stainless steel, the tubes **98** and **100** are attached to the housing **78** by silver solder. When made of plastic, the tubes **98** and **100** are adhesively bonded to the housing **78**.

[0062] It is possible to simultaneously apply more than two fluids and/or medical instruments to a target area. This is accomplished by a Verres needle **20'** as shown in FIGS. 10-13. In this embodiment, the Verres needle **20** of FIGS. 1-7 is altered so that a third port, such as stopcock **102**, is attached to the lumen housing **28'** via a threaded attachment. The stopcock **102** has an opening **104** that is in fluid communication with the portion B of central channel **30** of the lumen housing **28'**. The stopcock **102** allows for a third fluid to be received by the Verres needle **20'**. Note that lumen housing **28'** of FIG. 10 differs from lumen housing **28** of FIG. 1 in that the lumen housing **28'** is lengthened to accommodate the extra stopcock **102** and so a portion E of channel **30** connecting portions A and B is added.

[0063] Isolation between the three fluids is accomplished in part by chambers **74** and **76** as described previously with respect to the Verres needle **20** of FIGS. 1-7. Isolation between the fluid received by stopcock **102** is accomplished by a stationary cannula wall **106** that is positioned within the needle cannula exterior housing **78**. The wall **106** is attached to obturator **88** proximally of the opening **104** of the stopcock **102**. As shown in FIGS. 12 and 13, the wall **106** is substantially cylindrical/annular in shape having a length of approximately 4.5 inches, an inner diameter of approximately 0.094 inches and an outer diameter of approximately 0.12 inches. The wall **106** and wall **88** define an annular chamber **108** therebetween. The annular wall **88** has a length of approximately 6.75 inches, an inner diameter of approximately 0.73 inches and an outer diameter of approximately 0.84 inches. The separation between walls **88** and **106** is approximately 0.041 inches.

[0064] Regarding the formation of the chambers **74** and **76**, the annular wall **90** has a length of approximately 7.28 inches, an inner diameter of approximately 0.134 inches and an outer diameter of approximately 0.165 inches. The housing **78** and the wall **90** are spaced from one another by approximately 0.041 inches.

[0065] In operation, the stopcock **102** is opened so that a fluid is received by the opening **104** and delivered into the portion E of channel **30**. The fluid then flows into portion A of channel **30** and into the chamber **108** positioned between walls **88** and **106**. The fluid then flows out of an opening **110** formed in wall **88**, exits out of the opening **84** of the housing **78** and flows into a target area, such as a body cavity. The opening **110** is aligned with the opening **84**.

[0066] When all three stopcock **54**, **72** and **102** are open at the same time, the fluids associated with the stopcocks flow within the Verres needle **20** do not intermingle within the needle **20** since the chambers **74**, **76** and **108** are isolated from one another so they are permanently not in fluid communication with one another. The fluids are then expelled out of the Verres needle **20'** into the target area so that the chambers **74**, **76** and **108** simultaneously are in fluid communication with the target area.

[0067] The Verres needle **20'** described above with respect to FIGS. 10-13 can be used in a variety of medical proce-

dures, such as those described previously with respect to the Verres needle of FIGS. 1-7. For example, a pressure relief valve 112 can be connected to any of the ports, such as stopcock 72 as shown in FIG. 14 so as to permit the escape of gas in case of an over pressure situation. Other functions that could be performed by stopcock 72 are applying suction to chamber 108 to remove a fluid, providing a filtered exit port to allow smoke removal during electro surgical procedures, positioning an endoscope or an instrument through one of the other ports.

[0068] It should be noted that the matrix of applications discussed previously with respect to the Verres needle 20 of FIGS. 1-7 is applicable to the Verres needle 20' of FIGS. 10-13 in that the stopcock 102 can perform any one of the applications in the column of the matrix simultaneously with any dual application combination for stopcocks 54 and 72 as defined by the matrix.

[0069] While the above description regards using isolated chambers 74, 76 and 108 that are annular and concentric, it is possible to replace the annular walls 88, 90 and 106 with separate and nonintersecting tubes 98, 100 and 114 that are shown in FIG. 15. The tube 98 extends from the opening 92 to the distal end of the housing 78. Tube 100 extends from the opening 80 to the distal end of the housing 78. Similarly, tube 114 extends from portion A of channel 30 to the distal end of the housing 78. The tubes 98, 100 and 114 are preferably made of stainless steel or plastic and have a diameter of approximately 0.098. When made of stainless steel, the tubes 98 and 100 are attached to the housing 78 by silver solder. When made of plastic, the tubes 98 and 100 are adhesively bonded to the housing 78.

[0070] Another embodiment of a Verres needle that uses separate and nonintersecting tubes is shown in FIGS. 16-18. In this embodiment, the Verres needle 20" varies from the Verres needle 20' of FIG. 10 in that the stopcock 72 is now attached to the main body 28 and a fourth stopcock 116 is attached to the main body 28 as well. Thus, four fluids can be received simultaneously by the needle 20". As shown in FIG. 18, the stopcocks 72, 102 and 116 are spaced from one another by approximately 120°. The stopcock 116 has a tube 118 that is connected to it and that extends to the distal end of the housing 78. The tube 118 has a length of approximately 4.9 inches and diameter of approximately 0.098 inches that is the same as tubes 100 and 114. As shown in FIG. 18, the tube 98 is centrally located within main body 28 and the remaining tubes 100, 114 and 118 are each spaced 0.040 inches from the center of tube 98 and are spaced 120° relative to one another.

[0071] The foregoing description is provided to illustrate the invention, and is not to be construed as a limitation. Numerous additions, substitutions and other changes can be made to the invention without departing from its scope as set forth in the appended claims. For example, the present invention can be applied to other insertion devices, such as trocars, where the trocar is inserted into an opening of an animal, such as a human patient, and the opening was formed by an instrument separate from the trocar. In addition, the invention can be used in many fields of medicine, such as minimally invasive surgery, arthroscopy, urology, neurology, gynecology, gastroenterology, general surgery, anesthesiology, cardiology and internal medicine.

We claim:

1. An insertion device comprising:

a housing;

a first port attached to said housing for receiving a first fluid;

a first chamber connected to said first port and positioned within said housing, wherein said first chamber has an opening that is in fluid communication with a target area;

a second port attached to said housing for receiving a second fluid; and

a second chamber connected to said second port and positioned within said housing, wherein said second chamber has an opening that is in fluid communication with said target area, wherein said first chamber and said second chamber are permanently not in fluid communication with one another and simultaneously are in fluid communication with said target area.

2. The insertion device of claim 1, further comprising an annular wall inserted within said housing, wherein said annular wall and said housing define said first chamber.

3. The insertion device of claim 2, further comprising a second annular wall inserted within said housing and within said annular wall, wherein said annular wall and said second annular wall define said second chamber.

4. The insertion device of claim 2, further comprising an annular wall inserted within said housing, wherein said annular wall defines said first chamber.

5. The insertion device of claim 4, further comprising a second annular wall inserted within said housing, wherein said annular wall does not define a volume of space that is common with any volume of space defined by said second annular wall.

6. The insertion device of claim 1, further comprising:

a third port attached to said housing for receiving a third fluid; and

a third chamber connected to said third port and positioned within said housing, wherein said third chamber has an opening that is in fluid communication with said target area, wherein said third chamber, said second chamber and said first chamber are permanently not in fluid communication with one another and simultaneously are in fluid communication with said target area.

7. The insertion device of claim 6, further comprising an annular wall inserted within said housing, wherein said annular wall and said housing define said first chamber.

8. The insertion device of claim 7, further comprising a second annular wall inserted within said housing and within said annular wall, wherein said annular wall and said second annular wall define said second chamber.

9. The insertion device of claim 8, further comprising a third annular wall inserted within said housing and within said second wall, wherein said third annular wall and said second annular wall define said third chamber.

10. The insertion device of claim 6, further comprising an annular wall inserted within said housing, wherein said annular wall defines said first chamber.

11. The insertion device of claim 10, further comprising a second annular wall inserted within said housing, wherein

said annular wall does not define a volume of space that is common with any volume of space defined by said second annular wall.

12. The insertion device of claim 11, further comprising a third annular wall inserted within said housing, wherein said third annular wall does not define a volume of space that is common with any volume of space defined by either said annular wall and said second annular wall.

13. The insertion device of claim 1, wherein said housing comprises a needle formed at one end thereof.

14. The insertion device of claim 6, wherein said housing comprises a needle formed at one end thereof.

15. The insertion device of claim 2, wherein said annular wall is movable relative to said housing.

16. The insertion device of claim 15, further comprising a spring that engages said annular wall and said housing.

17. The insertion device of claim 7, wherein said annular wall is movable relative to said housing.

18. The insertion device of claim 17, further comprising a spring that engages said annular wall and said housing.

19. The insertion device of claim 1, wherein a first gas is present within said first chamber and a second gas is present within said second chamber.

20. The insertion device of claim 19, wherein said first gas comprises carbon dioxide and said second gas comprises carbon dioxide.

21. The insertion device of claim 1, wherein said first fluid comprises carbon dioxide and said second fluid comprises an aerosolized medication.

22. The insertion device of claim 1, further comprising a pressure transducer in fluid communication with said first port.

23. The insertion device of claim 1, further comprising a pressure relief valve in fluid communication with said first port.

24. The insertion device of claim 1, further comprising a filter in fluid communication with said first port.

25. An insertion device comprising:

a housing means for receiving a first fluid and a second fluid;

a first port means for receiving a first fluid;

a first chamber means for being in fluid communication with a target area;

a second port means for receiving a second fluid; and

a second chamber means for being in fluid communication with said target area, wherein said first chamber and said second chamber are permanently not in fluid communication with one another and simultaneously are in fluid communication with said target area.

26. The insertion device of claim 25, wherein said first chamber means comprises an annular wall inserted within said housing means.

27. The insertion device of claim 26, wherein said second chamber means comprises a second annular wall inserted within said housing means.

28. The insertion device of claim 27, wherein said annular wall does not define a volume of space that is common with any volume of space defined by said second annular wall.

29. The insertion device of claim 25, further comprising: a third port means for receiving a third fluid; and

a third chamber means for being in fluid communication with said target area, wherein said third chamber means, said second chamber means and said first chamber means are permanently not in fluid communication with one another and simultaneously are in fluid communication with said target area.

30. The insertion device of claim 29, wherein said first chamber means comprises an annular wall inserted within said housing means.

31. The insertion device of claim 30, wherein said second chamber means comprises a second annular wall inserted within said housing means.

32. The insertion device of claim 31, wherein said third chamber means comprises a third annular wall inserted within said housing means and within said second annular wall, wherein said third annular wall and said second annular wall define said third chamber means.

33. The insertion device of claim 25, wherein a first gas is present within said first chamber means and a second gas is present within said second chamber means.

34. The insertion device of claim 33, wherein said first gas comprises carbon dioxide and said second gas comprises carbon dioxide.

35. The insertion device of claim 25, wherein said first fluid comprises carbon dioxide and said second fluid comprises an aerosolized medication.

36. The insertion device of claim 25, further comprising a pressure transducer in fluid communication with said first port means.

37. The insertion device of claim 25, further comprising a pressure relief valve in fluid communication with said first port means.

38. The insertion device of claim 25, further comprising a filter in fluid communication with said first port means.

39. A method of treatment of a body cavity of an animal, comprising:

inserting a portion of an insertion device into a body cavity of an animal;

simultaneously receiving at said inserted insertion device a first fluid and a second fluid, wherein said first fluid and said second fluid are not in fluid communication with one another within said insertion device.

40. The method of claim 39, wherein said inserting comprises piercing of said animal with said insertion device.

41. The method of claim 39, further comprising:

forming an opening in said animal with an instrument separate from said insertion device; and

wherein said inserting comprises inserting said insertion device into said opening.

42. The method of claim 40, further comprising determining whether or not said portion of said insertion device is positioned with said body cavity.

43. The method of claim 40, wherein said process of simultaneously supplying further comprises simultaneously supplying from said inserted insertion device a third fluid into said body cavity, wherein said first fluid, said second fluid and said third fluid are not in fluid communication with one another within said insertion device.

44. The method of claim 39, wherein said first fluid comprises an insufflation gas and said second fluid comprises a fluid from a body cavity.

45. The method of claim 39, further comprising measuring the pressure of said first fluid.

46. The method of claim 39, further comprising relieving the pressure of said first fluid.

47. The method of claim 39, further comprising filtering said first fluid.

48. A method of treatment of a body cavity of an animal, comprising:

inserting a portion of an insertion device into a body cavity of an animal;

simultaneously receiving in said inserted insertion device a fluid and a medical instrument, wherein said fluid and said medical instrument are not in fluid communication with one another within said insertion device.

49. The method of claim 48, wherein said inserting comprises piercing of said animal with said insertion device.

50. The method of claim 49, further comprising:

forming an opening in said animal with an instrument separate from said insertion device; and

wherein said inserting comprises inserting said insertion device into said opening.

51. The method of claim 49, further comprising determining whether or not said portion of said insertion device is positioned with said body cavity.

52. The method of claim 48, wherein said fluid comprises an insufflation gas and said medical instrument is selected from the group consisting of a catheter, a grasper or an endoscope.

53. The method of claim 49, further comprising measuring the pressure of said fluid.

54. The method of claim 48, further comprising relieving the pressure of said fluid.

55. The method of claim 48, further comprising filtering said fluid.

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摘要(译)

一种治疗动物体腔的方法，包括将插入装置的一部分插入动物的体腔中，同时从插入的插入装置向第一液体和医疗器械或第二液体供给体内腔，其中第一流体和医疗器械或第二流体在插入装置内不彼此流体连通。

