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(54) **DEVICE FOR MAINTAINING
VISUALIZATION WITH SURGICAL SCOPES**

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A61B 1/12 (2006.01)
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CPC *A61B 1/127* (2013.01); *A61B 1/00091* (2013.01); *A61B 1/00135* (2013.01); *A61B 1/126* (2013.01)

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See application file for complete search history.

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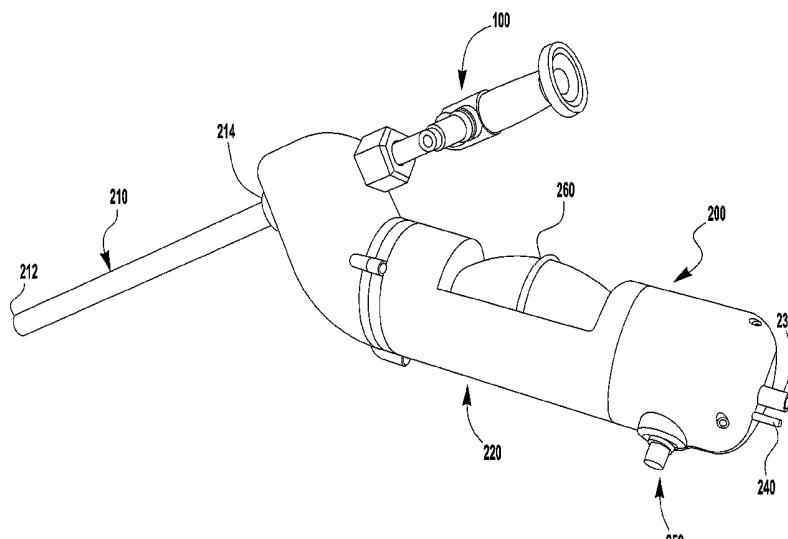
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(57) **ABSTRACT**

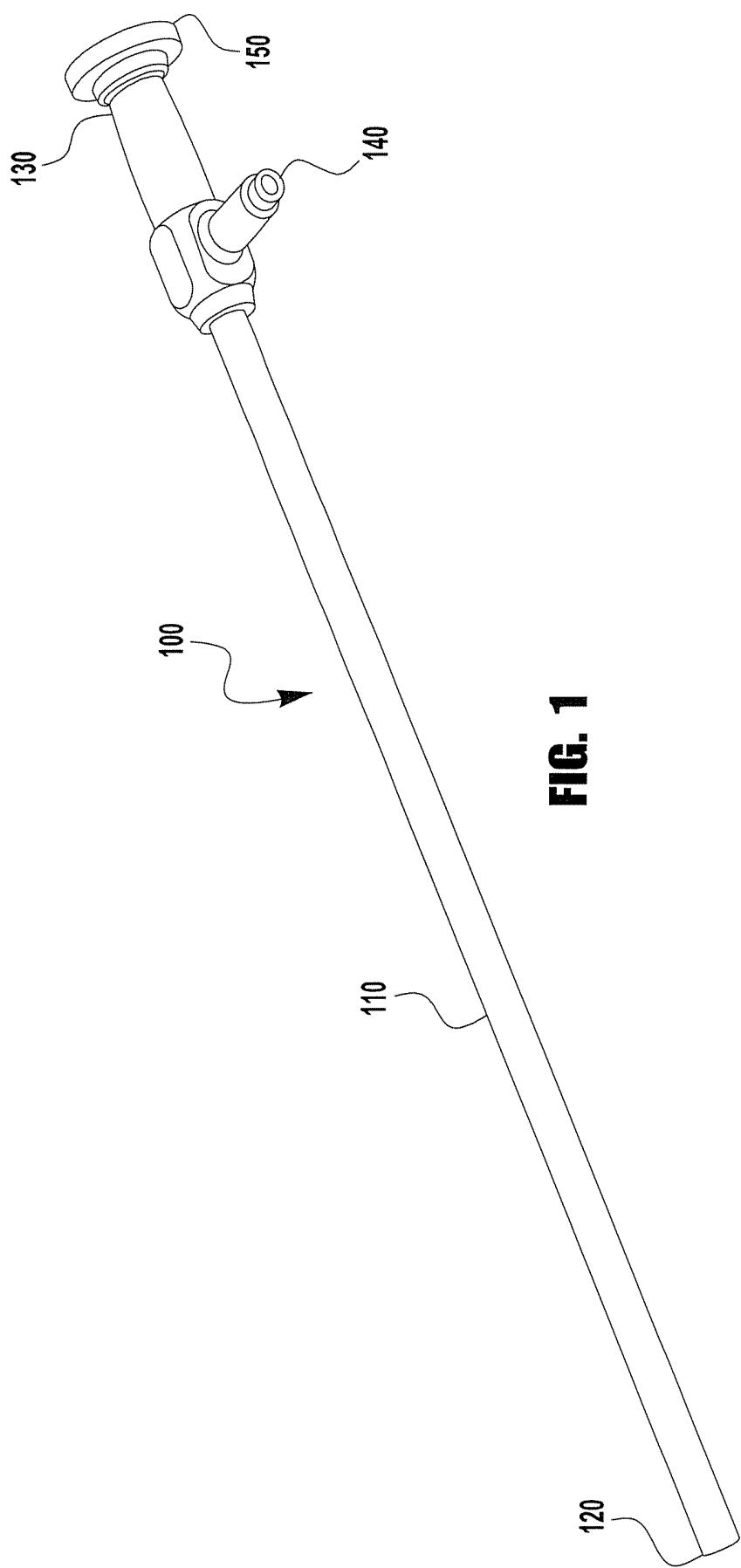
The present application discloses several embodiments of a devices for maintaining visualization with a surgical scope. The embodiments of the device are adapted to shield, defog or clean the lens of the surgical scope while the surgical scope is being used to perform a surgical procedure within a patient's body. In one embodiment, a view optimizer is provided that is adapted to deliver at least one fluid to the objective lens of the laparoscope to clean and/or defog the objective lens of the laparoscope without the need to remove the laparoscope from the surgical field. In additional embodiments, a view optimizer is provided that is adapted to create leakage or venting of gas from the body cavity so as to ensure continuous gas flow from an insufflator.

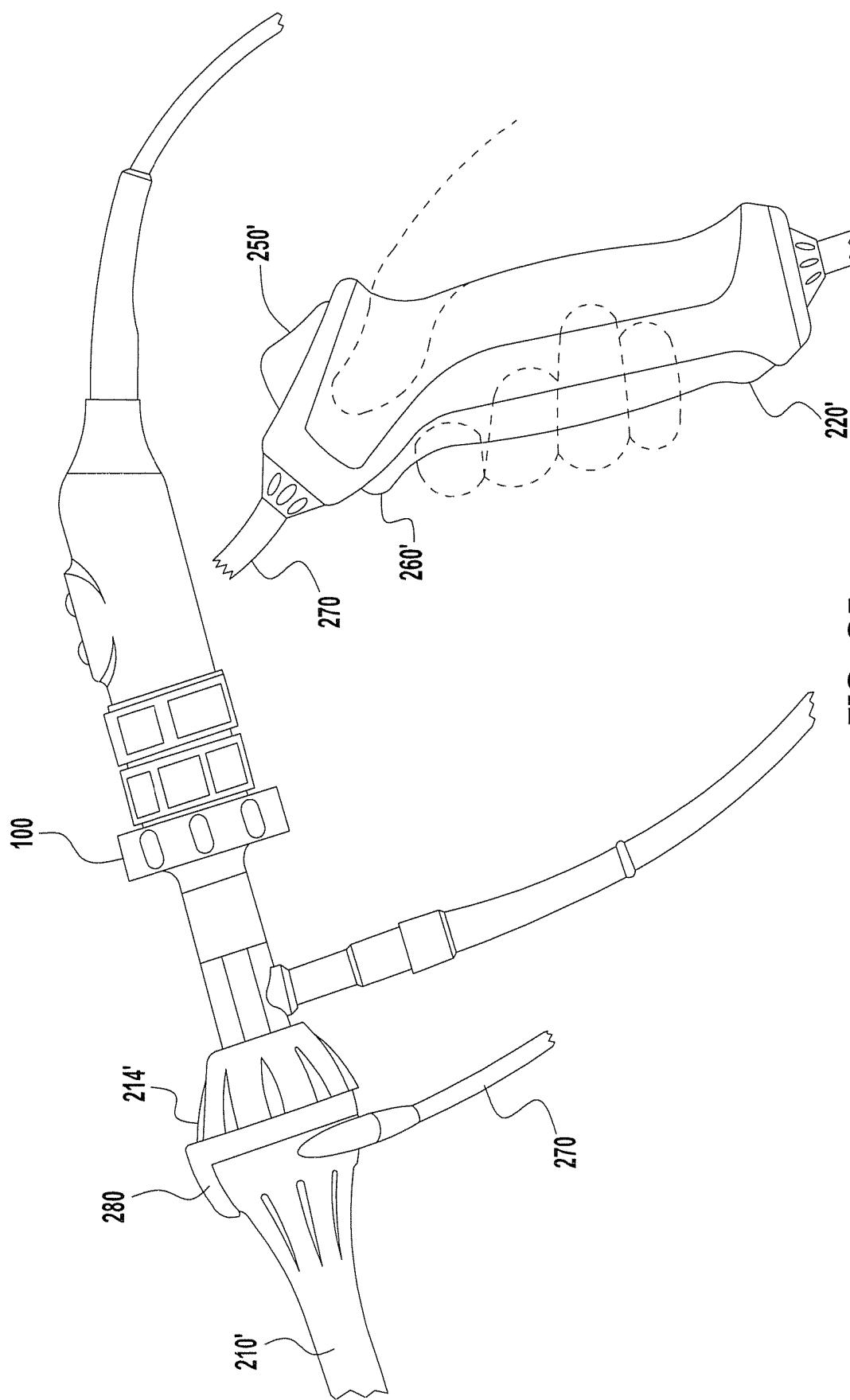
7 Claims, 9 Drawing Sheets

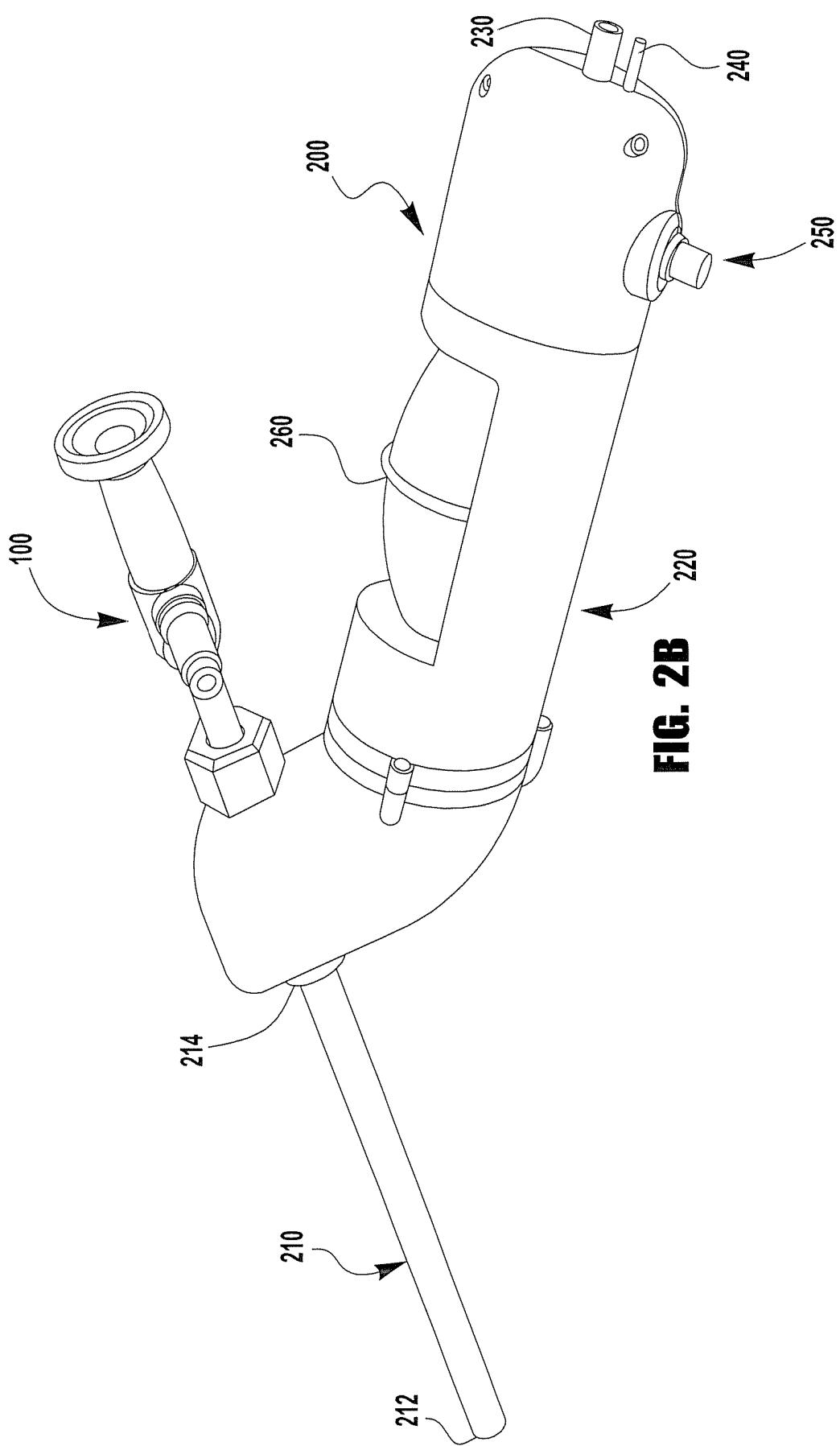


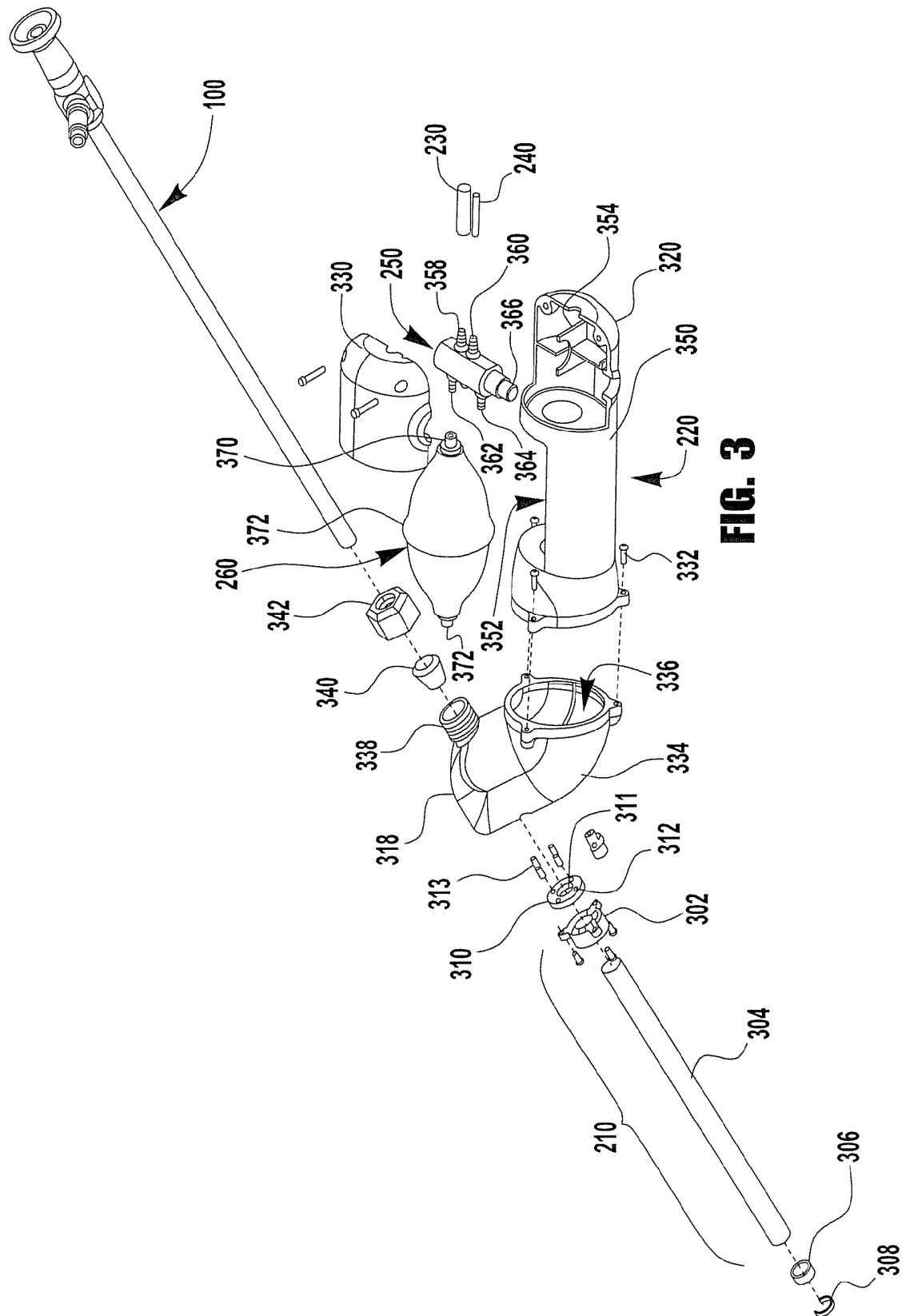
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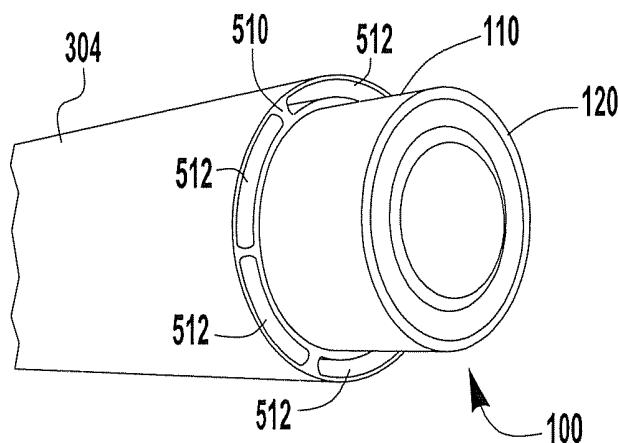
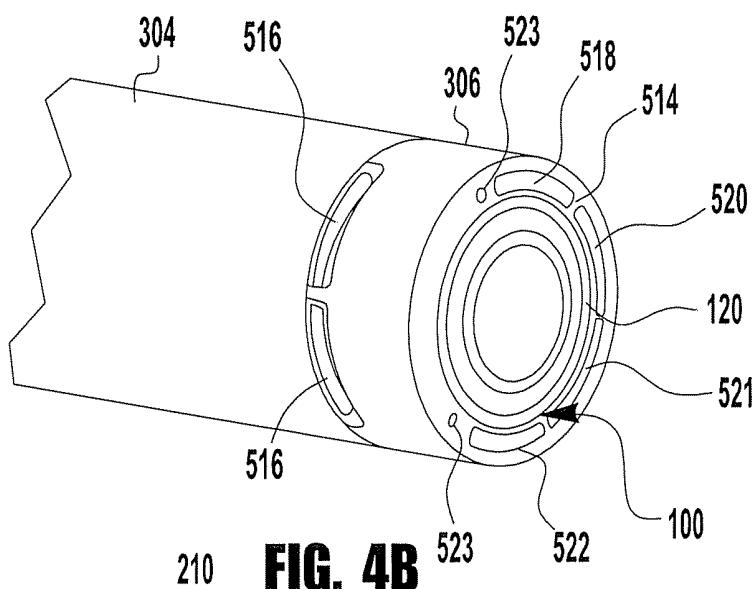
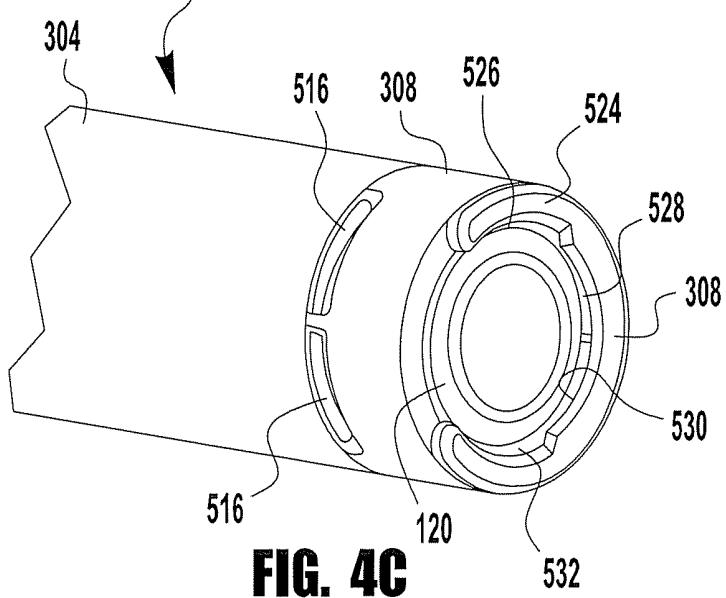
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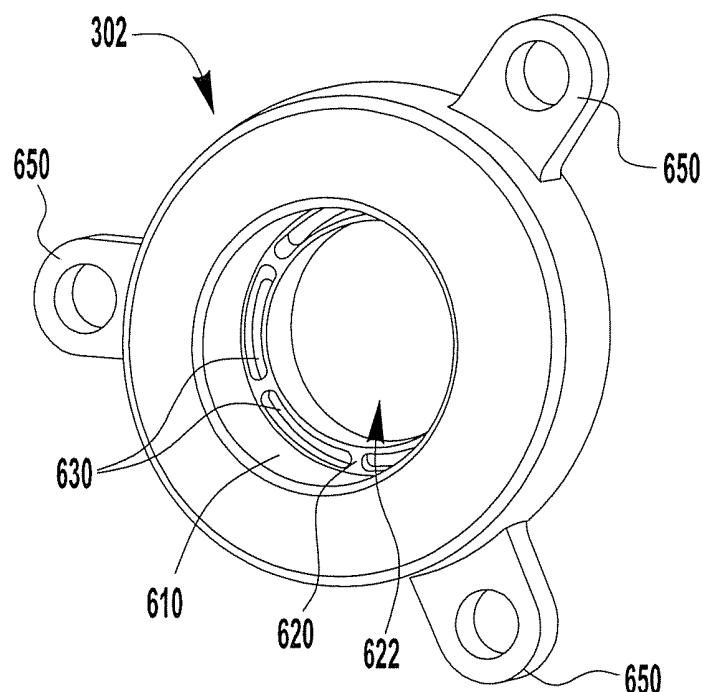
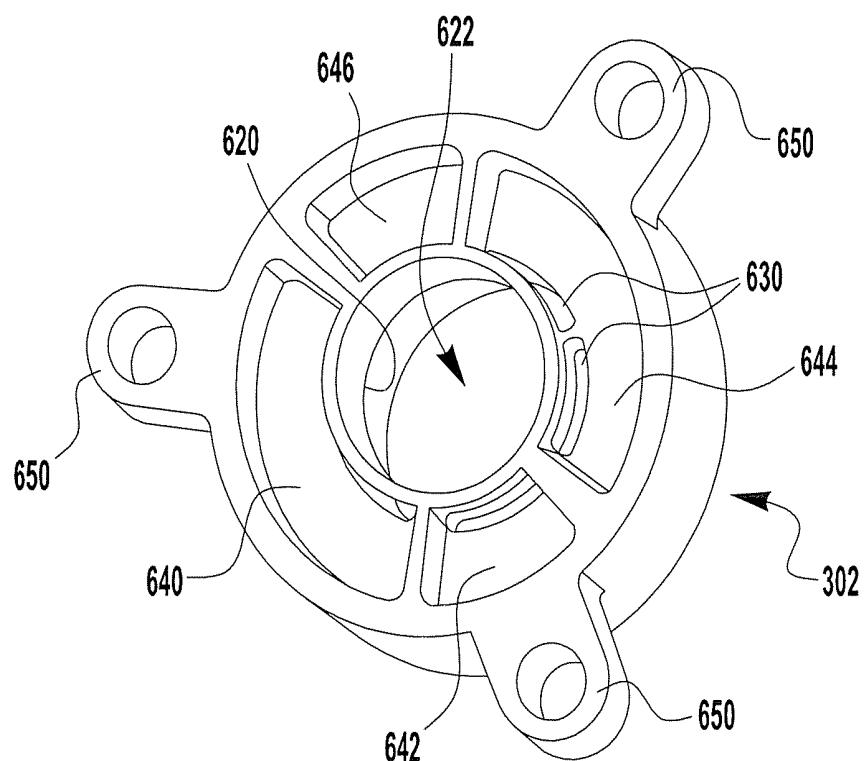


**FIG. 2A**





**FIG. 4A****FIG. 4B****FIG. 4C**

**FIG. 5A****FIG. 5B**

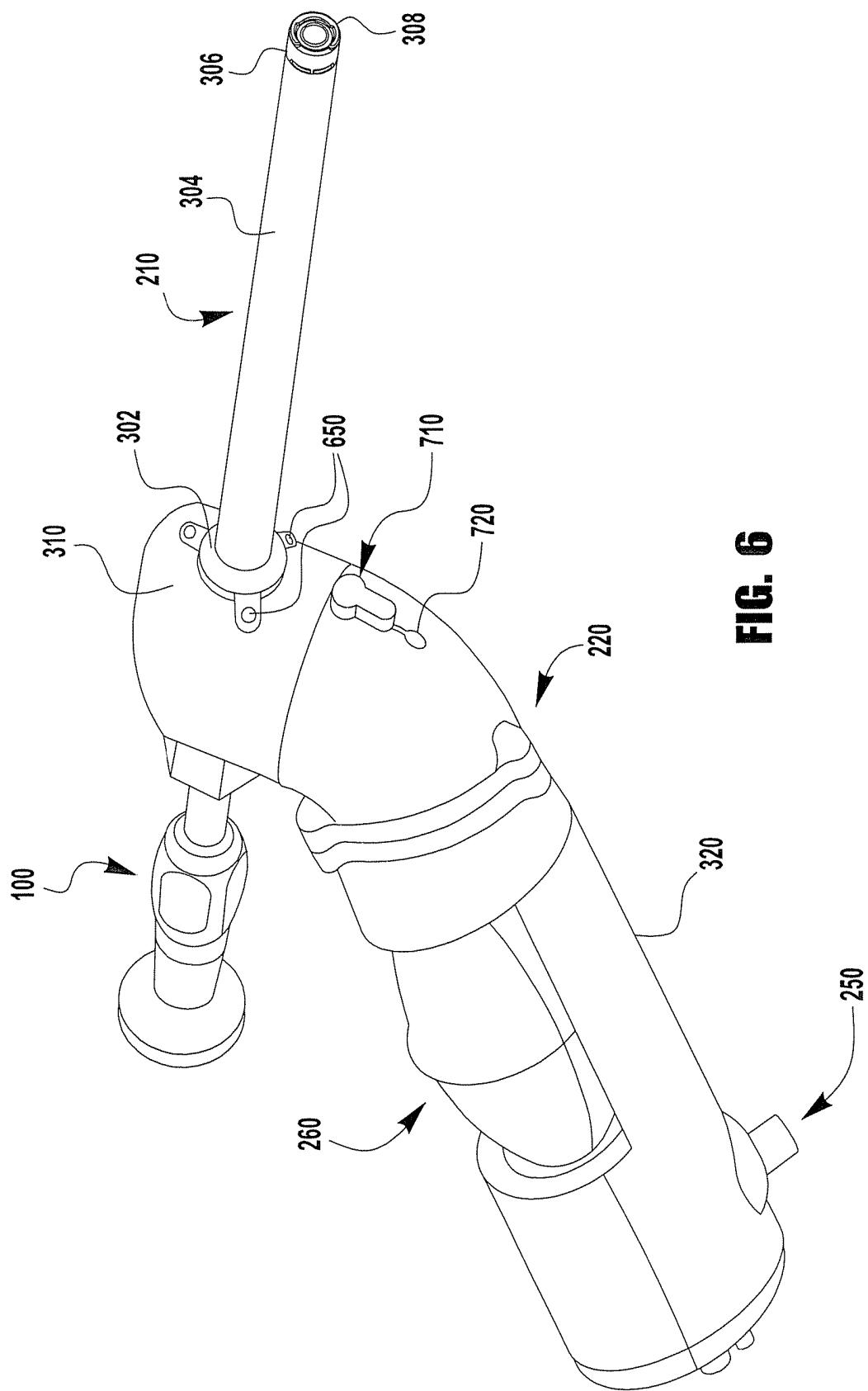
**FIG. 6**

FIGURE 7
Scope Temperature Distribution, Dry Tip Wipe

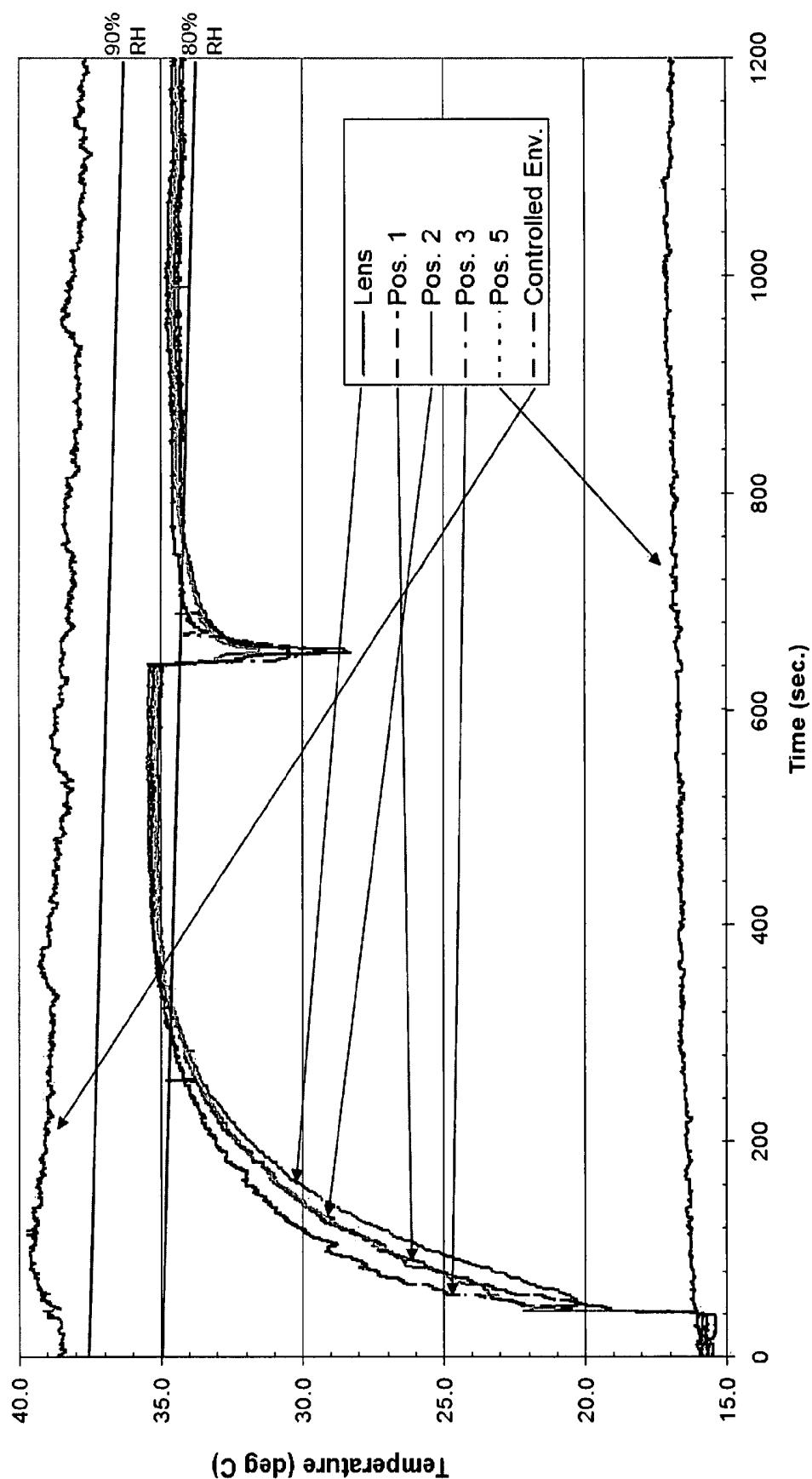
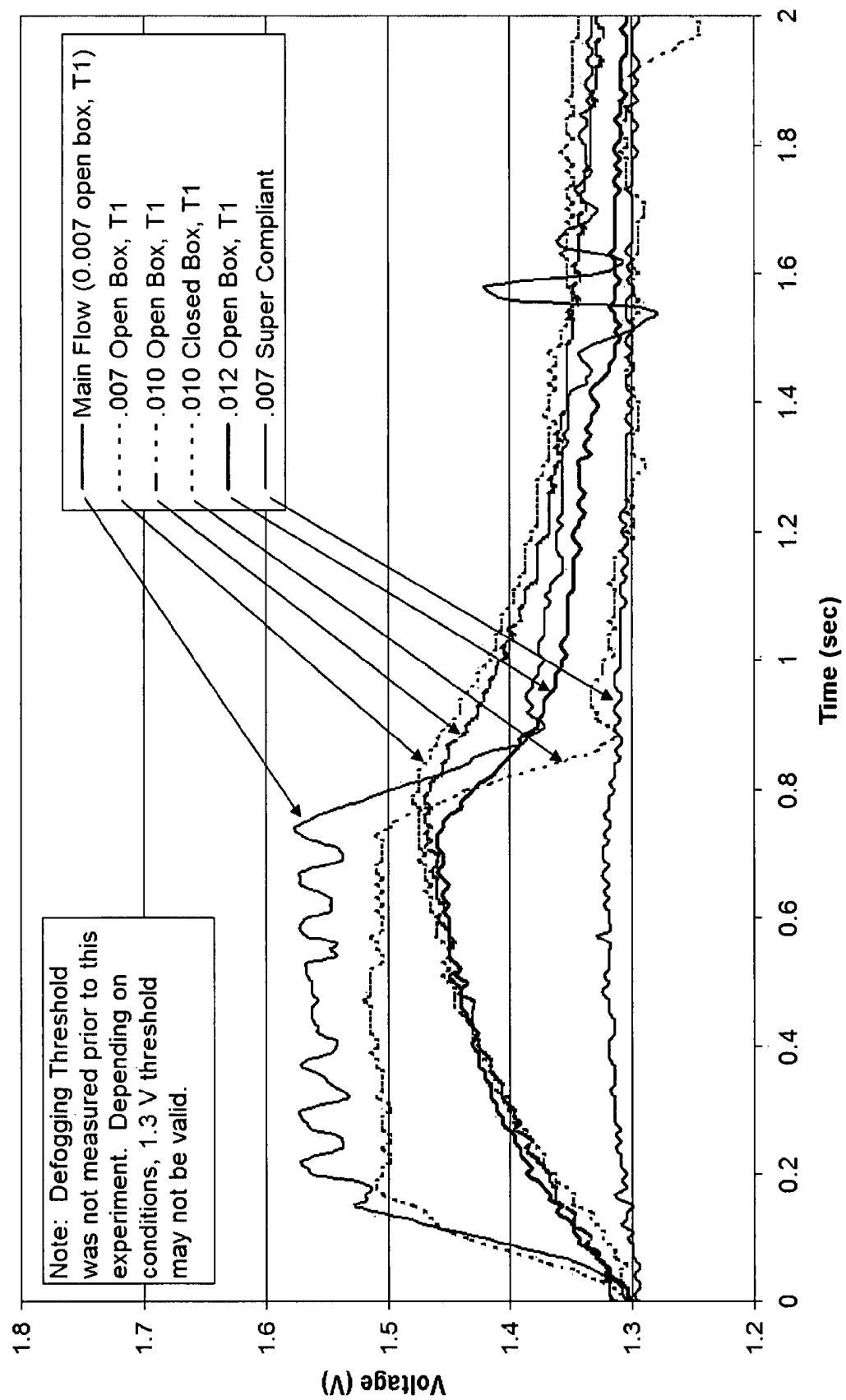


FIGURE 8



DEVICE FOR MAINTAINING VISUALIZATION WITH SURGICAL SCOPES

TECHNICAL FIELD

The present application relates generally to various embodiments of a device for maintaining visualization with surgical scopes. More particularly, this application relates to various embodiments of a view optimizer adapted to shield, clean and de-fog the defog or clean lens of a surgical scope, such as a laparoscope, while the surgical scope is being used to perform a surgical procedure within a cavity of a patient's body.

BACKGROUND OF THE INVENTION

Minimally invasive surgical procedures utilizing surgical scopes are desirable because they often provide one or more of the following advantages: reduced blood loss; reduced post-operative patient discomfort; shortened recovery and hospitalization time; smaller incisions; and reduced exposure of internal organs to possible contaminants.

Generally, minimally invasive surgeries utilize scopes, such as laparoscopes, that permit remote visualization of a surgical site within a patient's body while the surgical procedure is being performed. During a laparoscopic procedure, the patient's abdominal or pelvic cavity is accessed through two or more relatively small incisions rather than through a single large incision that is typical in a conventional surgery. Surgical scopes, such as laparoscopes, usually consist in part of a rigid or relatively rigid rod or shaft having an objective lens at one end and an eyepiece and/or integrated visual display at the other. The scope may also be connected to a remote visual display device or a video camera to record surgical procedures.

In laparoscopic surgeries, the abdomen is typically inflated with a gas through the use of an insufflator, to distend the abdominal space by elevating the abdominal wall above the internal organs and thereby create a sufficient working and viewing space for the surgeon. Carbon dioxide is usually used for insufflation, though other suitable gases may also be used. Conventional insufflators are adapted to cycle on and off to maintain a preset and suitable pressure within the patient's body cavity.

The local environment within a patient's abdominal space is generally rather warm and humid, and the use of devices such as harmonic scalpels and other cutting and coagulating devices generate mist, smoke, and other debris that is released into the surgical field and often becomes suspended throughout the expanded abdominal space. Additionally, blood, bodily fluids, pieces of tissue, fat or other bodily material may come in contact with or even attach to the lens. As a result of these conditions, visualization through the scope can be significantly diminished. Typically, the only solution to fogging and debris collection on the lens is removal of the scope from the body cavity and defogging or cleaning the lens by wiping it with a cloth, warming the scope tip, or utilizing another defogging method. The need to remove the scope to defog and remove debris from the lens is inconvenient for the scope operator and the surgeon and can interrupt and undesirably prolong surgical procedures.

SUMMARY

Embodiments of a device for maintaining visualization with a surgical scope are provided. The embodiments of the device are adapted to shield, defog or clean the lens of the

surgical scope while the surgical scope is being used to perform a surgical procedure within a patient's body.

Additional features and advantages of the invention will be set forth in part in the description which follows, and in part will be obvious from the description, or may be learned by practice of the invention. The features and advantages of the invention will be realized and attained by means of the elements and combinations particularly pointed out in the appended claims.

It is to be understood that both the foregoing general description and the following detailed description are exemplary and explanatory only and are not restrictive of the invention, as claimed.

The accompanying drawings, which are incorporated in and constitute a part of this specification, illustrate several embodiments of the invention, and together with the description, serve to explain the principles of the invention.

BRIEF DESCRIPTION OF THE DRAWINGS

The present invention may be more readily understood by reference to the following drawings wherein:

FIG. 1 is a perspective view of a laparoscope;

FIG. 2A is a perspective view of a first embodiment of a the laparoscope view optimizer in use with the laparoscope of FIG. 1;

FIG. 2B shows a side view of another exemplary embodiment of the view optimizer 200 of the present application;

FIG. 3 is an exploded perspective view of the view optimizer of FIG. 2;

FIG. 4A is a magnified perspective view of the guard tube of the view optimizer of FIG. 2A surrounding the laparoscope of FIG. 1;

FIG. 4B is a magnified perspective view of the guard tube and exhaust ring of the view optimizer of FIG. 2A surrounding the laparoscope of FIG. 1;

FIG. 4C is a magnified perspective view of the guard tube, exhaust ring and end ring of the view optimizer of FIG. 2A surrounding the laparoscope of FIG. 1;

FIG. 5A is a magnified front perspective view of the adapter ring of the view optimizer of FIG. 2;

FIG. 5B is a magnified rear perspective view of the adapter ring of the view optimizer of FIG. 2;

FIG. 6 is an alternate perspective view of the view optimizer of FIG. 2;

FIG. 7 shows results of analysis of humidity and fogging; and

FIG. 8 shows results of evaluation of effect of introduction of compliant accumulator on flow across laparoscope lens.

DETAILED DESCRIPTION OF THE INVENTION

The present invention will now be described with occasional reference to specific embodiments of the invention. This invention may, however, be embodied in different forms and should not be construed as limited to the embodiments set forth herein. Rather, these embodiments are provided so that this disclosure will fully convey the scope of the invention to those skilled in the art.

Except as otherwise specifically defined herein, all terms used herein have the same meaning as commonly understood by one of ordinary skill in the art to which this invention belongs. The terminology used in the description of the invention herein is for describing particular embodiments only, and is not intended to be limiting of the invention. As used in the description of the invention and the appended claims, the

singular forms "a," "an," and "the" are intended to include the plural forms as well, unless the context clearly indicates otherwise.

Unless otherwise indicated, all numbers expressing quantities, properties, and so forth as used in the specification and claims are to be understood as being modified in all instances by the term "about." Accordingly, unless otherwise indicated, the numerical properties set forth in the following specification and claims are approximations that may vary depending on the desired properties sought to be obtained in embodiments of the present invention. Notwithstanding that the numerical ranges and parameters setting forth the broad scope of the invention are approximations, the numerical values to the extent that such are set forth in the specific examples are reported as precisely as possible. Any numerical values, however, inherently contain certain errors necessarily resulting from error found in their respective measurements.

The present application relates generally to various embodiments of a device for use with surgical scopes. More particularly, this application relates to various embodiments of view optimizer devices of varying constructions for use with laparoscopes, the view optimizer device being adapted to shield, defog or clean the lens of the laparoscope while the laparoscope is being used to perform a surgical procedure within a patient's body. Though the device is referred to herein as a view optimizer, it will be appreciated that its designation as such is not intended to limit in any way its use and operation for a variety of purposes as further described herein in addition to controlling, improving and maintaining and improving desirable visualization of a laparoscopic surgical field.

Referring to FIG. 1, a perspective view of an exemplary, conventional laparoscope 100 is shown. The laparoscope 100 has an elongated cylindrical main body 110 having a distal end 120 and an imaging end 130. The main body 110 of the laparoscope may be either rigid or flexible, depending on the procedure the laparoscope is being used to perform, as well as the type of laparoscope being utilized. An objective lens (not shown in FIG. 1) is disposed within the distal end 120 of the main body 110, the objective lens being generally transverse to the longitudinal axis of the main body 100. Generally, laparoscope 100 includes an illumination system, which can be any type of suitable illumination system, such as a network of fiber optic cables, housed within the main body 110 of laparoscope 100 for illuminating the surgical site being imaged by the operative lens of the laparoscope. Laparoscope 100 includes an illuminator connector 140 for the connection of an external light source, which supplies the illumination system with illuminating light.

The imaging end 130 of the main body 110 includes an eyepiece 150. Conventional laparoscopes include an image transmission system (not shown in FIG. 1), which can be any type of suitable image transmission systems, such as a system of lens, lens rods or other optical components, housed within the main body 110 of the laparoscope for transmitting the image viewed by the objective lens to the eyepiece 150, thus allowing the scope operator to view within the patient's abdominal cavity. It is well known in the art that a video camera or other visual display device can be operatively connected to the eyepiece 150 or other portion of the laparoscope 100 to convert the optical signal into a video signal, which is ultimately processed by a video processing means to produce a video image on a monitor or for storage on magnetic tape or other storage media. It should be understood that the laparoscope discussed above is representative of conventional laparoscopes. It will be appreciated that in its various embodiments, the view optimizer device of the present appli-

cation can be used in connection with a variety of laparoscopes or other surgical scopes of varying constructions.

Referring now to FIG. 2, a perspective view of an exemplary embodiment of the view optimizer 200 of the present application is represented. As shown in FIG. 2, the view optimizer 200 generally includes a lens guard 210 and a flow controller 220. The lens guard 210 of the illustrated embodiment is adapted to receive a portion of the laparoscope 100, most particularly the distal end 120 thereof, and a portion of the main body 110 of the laparoscope. The lens guard 210 of the illustrated embodiment is in the form of a substantially continuous cylindrical sheath or tube that encloses a significant portion of the body of the laparoscope 100. It will be appreciated that in alternate embodiments, the lens guard 210 may be discontinuous, such that it may be formed of an open lattice or matrix that does not fully enclose the body of the laparoscope. As will be described further herein, the common structural features of the various embodiments of the lens guard 210 will be adapted to allow communication between the lens guard 210 of the view optimizer 200 at the distal end 120 of the laparoscope, on the one hand, and the flow controller 220 of the view optimizer 200 on the body 110 of the laparoscope near its imaging end 130, on the other hand, so as to provide for the functions of the view optimizer. Referring again to FIG. 2, the illustrated view optimizer 200 is adapted to deliver to the objective lens of the laparoscope at least one fluid selected from, for example, a liquid, such as water or saline, and a gas, such as CO₂ or air, to prevent the contact of material with the objective lens of the laparoscope or to defog or clean the objective lens of the laparoscope without the need to remove the laparoscope from the surgical field.

According to some embodiments, the view optimizer 200 is adapted to deliver a stream of fluid to the objective lens of the laparoscope so as to create a current passing over the face of the lens that transports moisture located on or near the lens away from the lens, thus preventing moisture from adhering to the lens. In additional embodiments, the view optimizer 200 delivers a stream of fluid to the objective lens at a temperature that is adapted to help ensure that the temperature of the objective lens does not fall to a point that is at or below the dew point temperature within the patient's abdominal cavity, thus preventing condensation from forming on the lens. Finally, in yet additional embodiments, the view optimizer 200 is adapted to deliver a stream of generally anhydrous fluid to the objective lens. In such embodiments, the generally anhydrous fluid serves to attract and absorb moisture particles located on or near the lens and carry the moisture away from the lens with the flow of fluid. Medical grade CO₂ for use with conventional insufflators is typically 99% pure, that is, no more than 1% of the gas is other than CO₂, and such medical grade CO₂ generally has a maximum moisture content of 25 parts per million by volume.

It should be understood that additional embodiments of the view optimizer 200 may perform only one of the above-described functions or any combination of these functions. Based on testing that was conducted in connection with the view optimizer 200 of the illustrated embodiment, when the temperature within the patient's abdomen was approximately 102.9° F. and the relative humidity within the patients abdomen was 76%, the delivery of a stream of fluid to the objective lens of the laparoscope 100 at a flow rate of equal to or greater than 0.07 liters per minute proved to be effective for defogging the lens (and/or preventing the fogging of the lens). It should be understood, however, that a variety of different flow rates will be effective for defogging the lens depending on the temperature and the moisture content of the gas being supplied by the insufflator and the temperature and relative

humidity of the patient's abdomen as well as other variables. As a way of illustrating the defogging effects of the view optimizer 200 according to one embodiment, the following information was collected regarding the dew point temperature of the objective lens of the laparoscope when located within the patient's abdominal cavity.

According to some embodiments, the view optimizer 200 is adapted to deliver a stream of one or more fluids across the objective lens of the laparoscope 100 to deflect blood, bodily fluids, pieces of tissue, fat or other bodily material that come within the vicinity of the objective lens. The stream of fluid may be either continuous or intermittent. In addition, according to some embodiments, the view optimizer 200 is adapted to deliver a burst or bolus of gas and/or liquid to the objective lens of the laparoscope when the scope operator desires. This burst or bolus of gas and/or liquid serves, at least in part, to facilitate removal of blood, bodily fluids, pieces of tissue, fat or other bodily material on the objective lens. In this manner, the scope operator can deliver a burst of gas or liquid to the objective lens to remove a piece of material or droplet of liquid, which was otherwise unable to be removed from the objective lens. It should be understood that additional embodiments of the view optimizer 200 may perform only one of the above-described functions or any combination of these functions.

The gas that is delivered to the objective lens of the laparoscope 100 by the view optimizer 200 is supplied by a conventional insufflator. Of course, it should be understood that the view optimizer 200 of this application could be supplied with gas via another external source other than an insufflator, or could include a gas supply device incorporated within or provided with the view optimizer 200, or by combinations of gas sources. Conventional insufflators are designed to insufflate a patient's abdominal cavity until a pre-determined suitable pressure for the operative procedure is reached. Once this pre-determined pressure is reached, conventional insufflators are designed to cease insufflating the cavity. Typical insufflators are designed to resume insufflation once the pressure in the cavity drops below the pre-determined pressure due to the leakage of gas through the trocars being used, through incisions in the patient's body cavity, or by some other means. In this manner, conventional insufflators typically continuously cycle between an insufflation state and a static state while being utilized during an operative procedure to maintain a pre-determined pressure within the patient's abdominal cavity.

According to various embodiments, the view optimizer 200 delivers gas to the lens of the laparoscope so as to provide a guard or shield to deflect liquid and particulate debris and prevent it from contacting the lens. According to some embodiments, the gas delivery is intermittent. According to other embodiments, such as the embodiment illustrated in FIG. 2, the flow of gas is essentially continuous. As such, the flow of gas during operation of the view optimizer 200 flows constantly, with delays of flow that are of a duration not greater than 5 seconds. Accordingly, in various embodiments wherein the flow of gas is essentially continuous, delays in flow are of a duration that is not greater than about 0.2, 0.4, 0.6, 0.8, 1.0, 2, 3, 4, or 5 seconds. As is further described herein, the embodiment of the view optimizer 200 illustrated in FIG. 2A is supplied with gas by the insufflator comprises one or more of a variety of means to permit an essentially uninterrupted supply of gas to be directed across the objective lens of the laparoscope 100. Accordingly, the illustrated embodiment includes a leakage or venting of gas from the body cavity so as to ensure continuous gas flow from the insufflator. This leak allows gas to exit the patient's abdomi-

nal cavity as necessary to ensure that the insufflator remains substantially in an insufflation state, thus supplying the view optimizer 200 with a generally continuous supply of gas.

The leak of the illustrated embodiment is created by a vent 5 or vents defined within the lens guard 210. The leak of the illustrated embodiment of the view optimizer 200 is a controlled leak that can be controlled by a user of the scope through the use of a valve or other control mechanism. The valve provided to control the leak could be a simple two-state, 10 on/off valve or it could be a multi-state, variable valve that allows the flow rate of the leak to be adjusted. The valve or other control mechanism could be either manually operated or automated, or under electronic control. Thus, it should be understood that the leak created by the view optimizer 200 15 could be provided in a manner that is not controlled by a user.

The view optimizer 200 of the illustrated embodiment provides a leak that has a flow rate that is generally between zero (0) and eight (8) liters per minute, and approximately 7.8 liters per minute, wherein two of the six channels are for 20 exhaust venting (as discussed further herein in connection with FIG. 4). Accordingly, in various embodiments, the flow rate of the leak is about 0, 0.5, 1, 1.5, 2.0, 2.5, 3.0, 3.5, 4.0, 4.5, 5.0, 5.5, 6.0, 6.5, 7.0, 7.5, 8.0 liters per minute. However it should be understood that additional embodiments of the 25 view optimizer 200 may provide a leak having a variety of different flow rates, in which case such flow rates may exceed 8, 9, 10, 12, 14, 16, 18, or more liters per minute, or increments thereof. As a way of illustrating the effect of the leak provided by the view optimizer 200 of the illustrated embodiment on the insufflator, the following information was collected regarding the cycling intervals of a conventional insufflator during an operative procedure when a leak was provided by the view optimizer as compared to the insufflator operating without a leak being provided.

In addition, while the leak created by the view optimizer 200 of the illustrated embodiment is a passive leak that relies on the pressure within the patient's body cavity to expel gas from within the cavity, alternative embodiments of the view optimizer could be augmented by the utilization of a vacuum 40 or other suction means to create a suction force that actively draws gas out from within the patient's body cavity. In such embodiments, the leak could likewise be under the control of the user, or otherwise under the control of an automated source or an electronic control.

Such embodiments that provide a vacuum or other suction means, may provide a suction force between zero (0) inches of mercury (in. Hg) and twenty six (26) inches of mercury (in. Hg). Accordingly, in various embodiments, the suction force provided is about 0, 1, 2, 3, 4, 5, 6, 7, 8, 9, 10, 11, 12, 13, 14, 15, 16, 17, 18, 19, 20, 21, 22, 23, 24, 25 or 26 inches of mercury (in. Hg). In some embodiments the suction force provided by the vacuum or other suction means of such embodiments is between twelve (12) inches of mercury (in. Hg) and fourteen (14) inches of mercury (in. Hg). However it should be understood that additional embodiments of the view optimizer 200 may provide a suction force having a variety of values that exceed 26 inches of mercury.

In additional embodiments of the view optimizer 200, the controlled leak could be created in alternative ways other than vents defined within the lens guard 210. For example, the leak could be created by a vent defined within the interface between the view optimizer 200 and the trocar that receives the view optimizer 200. For instance, the outer diameter of the lens guard 210 could be adapted to create a gap between the outer diameter of the lens guard 210 and the inner diameter of the trocar opening, thus, creating a leak. In addition, one or more notches, indentations or other openings could be

defined within the portion of the view optimizer 200 that interfaces with the trocar, or, alternatively, within a portion of the trocar that interfaces with the view optimizer 200, to create a gap through which gas could escape. Additional embodiments may include one or more notches, indentations or openings that extend along the entire length of the lens guard 210, thereby, creating a leak between the lens guard 210 and the trocar. As discussed previously, it should be understood that this leak located at the interface between the view optimizer 200 or lens guard 210 and the trocar could be controlled with the use of a valve or other control mechanism. In addition, this leak could be a passive leak or could utilize a vacuum or other pumping means to actively draw gas out from within the patient's body cavity. It will be appreciated that the construction of the lens guard 200 may be adapted such that whether it is formed as continuous sheath, or is formed of two or more portions, it is nevertheless adapted to allow for the introduction and control of a leak according to the various embodiments described herein.

While the creation of a leak helps to ensure that the insufflator provides the view optimizer 200 with a generally continuous supply of gas, the leak can also serve to remove moisture from within the patient's body cavity, thereby, decreasing the humidity within the cavity. Humidity levels in a laparoscopic surgical field can range from below 50% to close to 100% relative humidity; in most cases, the range is from about 75% to 99%, and most typically from about 85% to about 95%. Thus, the humidity within the abdomen can exist from less than 50%, to 55, 60, 65, 70, 75, 80, 85, 90, 95 and 100%, and increments thereof. Reduction of the humidity within the patient's body cavity serves to diminish the likelihood that the objective lens of the laparoscope 100 will become fogged when it is within the patient's body cavity. In addition, the leak can also help to remove smoke and mist generated from the use of a harmonic scalpel, and/or other particulate matter that is suspended in the gas within the patient's body cavity. This removal of airborne matter from within the patient's body cavity serves to ensure that the visibility through the objective lens of the laparoscope 100 is maintained.

It should be understood that the gas exiting the patient's body cavity via the leak created by the view optimizer 200 could be filtered in various embodiments. This filtering process could serve to remove blood, bodily fluids, or other matter from the gas exiting the patient's body cavity, thus, preventing these potential contaminants from entering the air within the operating room. It is beneficial to remove such matter from the escaping gas to prevent anyone in the operating room from inhaling such matter. It should also be understood that the gas exiting the patient's body cavity via the leak could be recycled for re-delivery into the patient's body cavity by the insufflator or the view optimizer 200. In addition, baffles or other muffling means could be incorporated with the vents provided by additional embodiments to muffle the sound of gas exiting the vents. Finally, it will be understood that in other embodiments, wherein the supply of fluid is to be intermittent, that there is not a need for a leak.

Referring again to FIG. 2, the lens guard 210 of the illustrated embodiment of the view optimizer 200 is an elongated, hollow cylindrical tube. The lens guard 210 has a distal end 212 and a proximal end 214. The distal end 212 of the lens guard 210 is adapted to surround the distal end 120 of the laparoscope 100. According to the illustrated embodiment, the distal end 212 of the lens guard 210 does not cover or fully enclose the distal end 120 of the laparoscope. It will be appreciated that in some alternate embodiments, a lens guard 210 may include structure that fully encloses the distal end

120 of the laparoscope, and as such is formed of a material that permits visualization. The proximal end 214 of the lens guard 210 is joined to the flow controller 220 of the view optimizer 200. The flow controller 220 of the view optimizer 200 of the illustrated embodiment is adapted to support and enclose components of the view optimizer 200. The flow controller 220 of the view optimizer 200 supplies the lens guard 210 with gas and/or liquid via one or more of conduits that connect to lens guard 210. The flow controller 220 receives gas and/or liquid from one or more exterior sources via air inlet 230 and liquid inlet 240 and delivers the gas and/or liquid to the lens guard 210. The flow controller 220 of the illustrated embodiment includes a gas/liquid flow actuator/regulator 250 for the actuation and/or regulation of the flow of gas and/or liquid to the lens guard 210. The flow controller 220 of the illustrated embodiment includes a burst flow actuator/regulator 260 for the actuation and/or regulation of the delivery of a burst or bolus of gas and/or liquid to the lens guard 210, as described above.

FIG. 2A shows the lens guard 210 and the flow controller 220 of the view optimizer 200 joined together as a unitary construction. It should be understood that the lens guard 210 and the flow controller 220 could be provided as two or more separate pieces that are used remotely from one another and not joined together as a unitary construction. FIG. 2B shows a side view of another exemplary embodiment of the view optimizer 200 of the present application. In this embodiment, the view optimizer 200 is in two separate pieces (the prime designation, e.g. 210', is used to reference features that are common between the embodiments depicted in FIG. 2A and FIG. 2B). The lens guard 210' is attached at its proximal end 214 to the laparoscope 100, and comprises a vent actuator 280, and a fluid conduit 270 that is in communication with the flow controller 220' (connection not shown). The flow controller 220' is depicted as an ergonomic device to be grasped in an operator's hand, with a flow actuator/regulator 250' adapted to be depressed by the operator's thumb, and a burst flow actuator/regulator 260' adapted to be depressed by the flexion of the operator's fingers, to deliver the flow of gas or liquid from one or more inlet sources (not shown) through the fluid conduit 270, for delivery to the objective lens of the scope through distal end 212 of the lens guard 210. In the depicted embodiment, the vent actuator 280 is under the control of the scope operator, and may be adjusted as needed to assist in maintaining visualization. Of course it will be understood that in alternate embodiments, one or more of three actuators may be eliminated, and their locations may be switched, or all actuators may be located on the flow controller 220' or may be located at yet another controller, such as a separate foot activated controller (not shown). In yet other embodiments, the lens guard 210 and the flow controller 220 could be provided as two or more separate pieces that are assembled for use. While the lens guard 210 and the flow controller 220 of the illustrated embodiment are formed from plastic, other suitable materials, such as metal or a composite material, or combinations of these could also be used.

Referring to FIG. 3, the view optimizer 200 will now be described with more particularity. As mentioned earlier, the lens guard 210 is an elongated, cylindrical tube. However, it should be understood that the lens guard 210 is not limited to this shape and configuration and other suitable shapes and configurations could also be used in additional embodiments. Examples of additional constructions have been previously described. Examples of additional cross-sectional shapes that could be used for the lens guard 210 include, but are not limited to, rectangular, triangular, oval, etc. The lens guard 210 can have any shape or configuration

which allows it to surround the distal tip 120 of the laparoscope 100. Additional embodiments of the view optimizer 200 may include a lens guard which has an angled portion to correspond with scopes with angled portions, such as 450 or 300 angled scopes. The lens guard 210 of the illustrated embodiment is substantially rigid. However, it should be understood that additional embodiments of the view optimizer may include a flexible lens guard, which is adapted for use with a flexible scope. The lens guard 210 of the embodiment illustrated in FIG. 2A is fashioned from plastic, but other suitable materials such as metal or a composite material or combinations of these could also be used.

While the view optimizer 200 of the illustrated embodiment includes a lens guard 210 that surrounds and encloses the entire length of the laparoscope 100, it should be understood that the lens guard 210 of the view optimizer 200 could have any shape, construction or configuration that allows it to deliver gas and/or liquid to the objective lens of the laparoscope 100. For example, in alternative embodiments the lens guard 210 could be formed of one or more channels, tubes or conduits adapted to deliver gas and/or liquid to the objective lens of the laparoscope 100. The channels, tubes or conduits of such embodiments of the lens guard 210 could be supported by a rigid or flexible framework. The channels, tubes or conduits of such embodiments could also be fastened to the laparoscope 100 itself, either removably or permanently, by one or more fasteners, such as straps, ties, adhesives, clips, etc. In such embodiments, additional methods of sealing the interface between the view optimizer 200 and the trocar may be employed. For example, the portion of the view optimizer 200 that interfaces with the trocar may be a member that serves to form a seal with the trocar while the portion of the view optimizer 200 that is inserted into the patient's body cavity and delivers gas and/or liquid to the objective lens of the laparoscope could be one or more channel, tube or conduit and/or a rigid or flexible framework. In addition, the lens guard 210 of additional embodiments could be adapted to surround and enclose only portions of the laparoscope 100, leaving other portions of the laparoscope 100 un-enclosed.

As shown in FIG. 3, the lens guard 210 of the illustrated embodiment includes an adapter ring 302, a guard tube 304, an exhaust ring 306, and an end ring 308. Referring to FIG. 4A, the guard tube 304 is shown with more particularity (the exhaust ring 306 and end ring 308 of the lens guard 210 are not present in FIG. 4A to better illustrate the construction of the guard tube 304). As shown in FIG. 4A, the guard tube 304 is a hollow, cylindrical tube adapted to surround the laparoscope 100. The guard tube 304 has an outer wall 510 that defines a hollow space. As shown in FIG. 4A, channels 512 are defined within the outer wall 510 and extend the length of the guard tube 304. The channels 512 are adapted to allow for the travel of gas and/or fluid along the length of the guard tube 318. The guard tube 304 depicted in the figures includes six channels 512, each having one or more functions. However, it should be understood that additional embodiments of the view optimizer may include any number of channels 512 defined within the guard tube 318, such as, for example, a single channel for multiple functions, or two or more channels each having distinct functions. The channels 512 may have a variety of sizes, shapes and configurations that allow for the passage of gas and/or liquid. The guard tube 318 of the illustrated embodiment shown in FIG. 5 has two channels 512 for the passage of exhaust gas from the interior of the patient's body cavity, and is suitable for providing a controlled leak. The illustrated embodiment also includes two channels dedicated to delivery of gas from the insufflator to the objective lens of the laparoscope 100, and one channel for the passage

of the liquid to the objective lens of the laparoscope. Additional embodiments of the view optimizer 200 may include guard tubes 304 that have any number of channels 512 dedicated to any combination of gas for delivery to the objective lens of the laparoscope, liquid for delivery to the objective lens of the laparoscope, and/or exhaust gas. As mentioned previously, various additional embodiments of the view optimizer 200 may utilize both gas and liquid or only one of gas or liquid for delivery to the objective lens of the laparoscope. In some embodiments, the view optimizer may lack exhaust channels. Generally, depending on the intended functionality of the lens guard, the one or multiple channels 512 of the guard tube 304 will be suitably adapted.

Referring to FIG. 4B, the guard tube 304 and exhaust ring 306 of the lens guard 210 are shown in use with a laparoscope 100 (the end ring 308 of the lens guard 210 is not shown in FIG. 4B to better illustrate the construction of the exhaust ring 306). The exhaust ring 306 is a hollow, cylindrical piece adapted to surround and enclose a portion of the laparoscope 100. As shown in FIG. 4B, the guard tube 304 and the exhaust ring 306 of the view optimizer 200 are attached together. The guard tube 304 and the exhaust ring 306 can be attached together in a variety of different ways, such as by adhesives, screws, tabs and slots, etc. In addition, the guard tube 304 and exhaust ring 306 could be formed together as a unitary construction.

The exhaust ring 306 has an outer wall 514 which defines a hollow space. Exhaust vents 516 are defined within the outer wall 514 of the exhaust ring 306. As shown in FIG. 4B, the guard tube 304 and the exhaust ring 306 abut against one another when the lens guard 210 is assembled. The exhaust vents 516 defined within the outer wall 514 of the exhaust ring 306 are adapted to form openings into two of the channels 512 of the guard tube 304 that are dedicated to the passage of exhaust gas from within the patient's body cavity in conjunction with the leak function of the view optimizer 200 of the illustrated embodiment. The pressure within the patient's body cavity is greater than the pressure within the channels 512 of the guard tube 304. Accordingly, gas from within the patient's body cavity will enter the exhaust vents 516 and travel through the channels 512 defined within the guard tube 304 out of and away from the patient's body cavity. While the embodiment of the exhaust ring 306 illustrated in FIG. 4B includes two exhaust vents 516, additional embodiments of the view optimizer 200 may include exhaust rings 306 with any number of exhaust vents. The exhaust vents 516 may have any shape, size and configuration which allows gas to enter the guard tube 306 or some other portion of the view optimizer 200. As discussed above, additional embodiments of the view optimizer 200 may lack a controlled leak function, thus, such embodiments of the view optimizer 200 will not include exhaust vents 516.

Referring again to FIG. 4B, channels 518, 520, 521 and 522 are defined within the outer wall 514 of the exhaust ring 306 and extend through the length of the exhaust ring 306. The channels are adapted to allow for the travel of either gas and/or liquid along the length of the exhaust ring 306. When the lens guard 210 is assembled, each of the channels 518, 520, 521 and 522 of the exhaust ring 306 align with a channel 512 of the guard tube 304 to allow for the passage of gas and/or liquid therethrough. While the exhaust ring 306 of the illustrated embodiment includes four channels, additional embodiments of the view optimizer may include exhaust rings 306 with any number of channels.

As depicted, channel 518 of the exhaust ring 306 of the illustrated embodiment is adapted for the passage of liquid for delivering to the objective lens of the laparoscope 100. Chan-

nels 520, 521 are adapted for the passage of gas for delivery to the objective lens of the laparoscope 100. Channel 522 of the exhaust ring 306 of the illustrated embodiments is not operative to allow for the passage of either gas and/or liquid. However, in additional embodiments, channel 522 could be functional. Channel 522 could act as an exhaust channel for both fluid and gas. While the exhaust ring 306 includes four channels, it should be understood that additional embodiments of the exhaust ring 306 may include any number of channels. The channels 518, 520, 521 and 522 may have a variety of sizes, shapes and configurations. The channels 518, 520, 521 and 522 can have any size, shape and configuration that allows for the passage of gas and/or liquid. As mentioned previously, various additional embodiments of the view optimizer 200 may utilize both gas and liquid or one of gas or liquid for delivery to the objective lens of the laparoscope for cleaning and/or defogging. Accordingly, such factors will determine the usage and number of channels as well as the construction, size, shape and configuration of the end ring 308 of additional embodiments of the view optimizer 200.

As shown in FIG. 4B, the exhaust ring 306 includes fastener openings 523 for use in the attachment of the end ring 308. As shown in FIG. 4C, the exhaust ring 306 and the end ring 308 of the view optimizer 200 are attached together. The exhaust ring 306 and the end ring 308 of the illustrated embodiment are attached together by projections (not shown) which extend from the end ring 308 and are received within the fastener openings 523 of the exhaust ring 306. However, it should be understood that the end ring 308 and the exhaust ring 306 can be attached together in a variety of different ways, such as by adhesives, screws, tabs and slots, etc. In addition, the end ring 308 and exhaust ring 306 could be formed together as a unitary construction.

Referring now to FIG. 4C the guard tube 304, exhaust ring 306 and end ring 308 are shown in use with a laparoscope 100. The end ring 308 is attached to the exhaust ring 306 and extends beyond the end of the laparoscope 100. This extension of the end ring 308 beyond the distal end 120 of the laparoscope 100 facilitates delivery of fluid to the lens, as further described herein, and helps to shield the objective lens from contacting objects or tissue, either within the patient's body cavity or outside of it, such as within the passageway within a trocar, that may soil, smudge, smear or adhere to the objective lens of the laparoscope. For example, conventional trocars include a seal assembly that consists of a plurality of flaps that create a seal with objects that are inserted through the trocar. These flaps of the trocar seal can become soiled with blood, bodily fluids, pieces of tissue, fat or other bodily material during an operative procedure. The extension of the end ring 308 beyond the distal end 120 of the laparoscope 100 serves to contact these flaps prior to the laparoscope 100 as the laparoscope 100 and view optimizer 200 are being inserted through the trocar, thereby deflecting the soiled flaps away from contacting the objective lens of the laparoscope 100, and thus, preventing any blood, bodily material or other matter that is on the flaps from contacting and/or dirtying the objective lens. Likewise, the extension of the end ring 308 beyond the distal end 120 of the laparoscope also serves to deflect objects, such as internal organs or other tissue or fat, from contacting the objective lens of the laparoscope 200 when within the patient's body cavity.

According to various embodiments, the end ring 308 portion of the view optimizer 200 may extend beyond the end of the laparoscope from about 0 mm to about 7 mm. Accordingly, in various embodiments, the end ring 308 portion of the view optimizer 200 may extend beyond the end of the laparoscope from about 0, 0.5, 1, 1.5, 2, 2.5, 3, 3.5, 4, 4.5, 5, 5.5, 6,

6.5, 7 mm or more. It should be understood that additional embodiments of the view optimizer 200 may not include an end ring 308 or other structure that extends beyond the distal end 120 of the laparoscope 100.

The end ring 308 is adapted to partially enclose the distal end 120 of the laparoscope 100. The end ring 308 has a main wall 524. Passageways 526, 528, 530 and 532 are defined within the main wall 524 of the end ring 308. Passageways 526, 528, 530 and 532 are adapted to direct the flow of gas and/or liquid exiting the channels 518, 520, 521 of the exhaust ring 306 across the operative lens of the distal end 120 of the laparoscope. The passageways 526, 528, 530 and 532 of the illustrated embodiment of the view optimizer 200 direct at least a portion of the flow of gas and/or liquid across the face of the objective lens. In the sheath assembly 200 of the illustrated embodiment, passageway 526 is adapted to direct the flow of liquid from channel 518 of the exhaust ring 306 across the objective lens of the laparoscope 100. Channels 528, 530 of the illustrated embodiment are adapted to direct the flow of the gas from channels 520, 521 of the exhaust ring 306 across the objective lens of the laparoscope 100 to deflect gas and liquid from the lens, defog the objective lens as well as to remove moisture or material from the surface of the objective lens. Channels 528, 530 are also adapted to direct at least a portion of the gas from channels 520, 521 in a path that projects forward from the objective lens (as viewed in FIG. 4C) at an angle relative to the objective lens. The flow of the gas that is directed forward from the distal end 120 of the laparoscope further serves to deflect away smoke, particulate, blood, bodily fluid, moisture, tissue, fat, or other material within the patient's body cavity from contacting the objective lens of the laparoscope 100. Accordingly, as the laparoscope 100 is inserted into the patient's body cavity and/or moved within the cavity, this forwardly projecting flow of gas serves to deflect away blood or other material that approaches the objective lens.

It should be understood that additional embodiments of the view optimizer 200 could direct all of the gas and/or liquid across the objective lens in a path that is generally parallel to the objective lens or could direct all of the gas and/or liquid in a path projecting forward and away from the distal end 120 of the laparoscope at an angle relative to the objective lens, or could direct all or a portion of the gas and/or liquid in a path projecting toward the distal end 120 of the laparoscope 100 at an angle relative to the objective lens, or any combination of parallel flow and angled flow.

Embodiments of the view optimizer 200 may provide for the delivery of gas and/or liquid in a path having any angle relative to the objective lens between 0° and 90° or between 0° and -90°, wherein the negative designation refers to paths directed toward the lens. In some embodiments, fins or louvers are provided to direct the flow of the gas and/or liquid in a variety of different paths each having a different angle relative to the objective lens, thereby, creating a fanned out flow of gas and/or liquid. According to various embodiments, the length of extension of the end ring 308 portion of the view optimizer 200 that extends beyond the end of the laparoscope from about 0 mm to about 7 mm may comprise one or more passageways that deliver a fluid stream at one or a range of positions along the length of the end ring 308. According to such embodiments, the passageways may be positioned at the base of the end ring 308, near to the lens of the scope, or at the distal end of the end ring 308, farthest away from the lens, or at one or more locations in between. And according to such various embodiments, the passageways may be configured to direct a narrow stream of fluid, or may be configured to direct a fan of fluid at various angles.

The embodiment depicted in FIG. 4C is configured with an end ring 308 that extends about 2 mm from the end of the laparoscope and is configured to deliver a fan of air at an angle of about 30°, thus the distance of the flow path nearest the lens at the point of the passageway is about 0 mm and the distance of the flow path nearest the lens at the opposite side of the lens is about 8 mm from the lens. Variation of the length of the end ring, distance of the passageway from the lens, angle or angles of flow may vary, such that the distance of the nearest flow path from the lens may range from 0 mm to more than 15 mm, and in some embodiments the flow path may be directed at an angle toward the lens.

The end ring 308 of additional embodiments can have a variety of sizes, shapes and configurations. The end ring 308, can have any size, shape or configuration that allows it to direct gas and/or liquid across the face of the objective lens of the laparoscope. While the end ring 308 of the illustrated embodiment only partially encircles the distal end 120 of the laparoscope 100, it should be understood that additional embodiments of the view optimizer 200 may include an end ring 308 that completely encircles the distal end 102 of the laparoscope 100. As mentioned previously, various additional embodiments of the view optimizer 200 may utilize both gas and liquid or one of gas or liquid for delivery to the objective lens of the laparoscope for cleaning and/or defogging. In addition, additional embodiments of the view optimizer 200 may not include a controlled leak function. Accordingly, such factors will affect the construction, size, shape and configuration of the end ring 308 of additional embodiments of the view optimizer 200.

Referring again to FIG. 3, an adapter ring 302 is located at the proximal end 214 of the lens guard 210. The adapter ring 302 is adapted to mount the lens guard 210 to the main body. The adapter ring 302 can have any size, shape or configuration that allows it to mount the lens guard 210 to the flow controller 220. In addition, as mentioned previously, the lens guard 210 and flow controller 220 of additional embodiments may be formed as a unitary piece or may also be located remotely from one another and not directly connected to one another.

As shown in FIG. 5A, the adapter ring 302 has a generally cylindrical shape with a guard tube opening 610 defined through it. The guard tube opening 610 is adapted to receive the guard tube 304. The guard tube opening 610 of the adapter ring has an inner rim 620. When the guard tube 304 is inserted into the adapter ring, the guard tube 304 abuts against the inner rim 620. In this manner, the inner rim 620 helps to properly locate the guard tube 304 within the adapter ring 302 and prevents the guard tube 304 from passing completely through the adapter ring 302. Several channels 630 are defined within the inner rim 620 of the adapter ring and pass through the length of the adapter ring 302. The adapter ring 302 of the illustrated embodiment of the view optimizer has six channels 630 to coincide with the six channels 512 of the guard tube 304. When the guard tube 304 is secured within the adapter ring 302, the channels 512 of the guard tube 304 align with the channels 630 of the adapter ring, to allow for gas and/or liquid to flow from the channels 512 of the guard tube to the coinciding channels 630 of the adapter ring 302 and vice versa.

While the adapter ring 302 of the illustrated embodiment includes six channels 630, it should be understood that additional embodiments of the adapter ring 302 may include any number of channels 630. The channels 630 may have a variety of sizes, shapes and configurations. The channels 630 can have any size, shape and configuration that allows for the passage of gas and/or liquid. As mentioned previously, vari-

ous additional embodiments of the view optimizer 200 may utilize both gas and liquid or one of gas or liquid for delivery to the objective lens of the laparoscope for cleaning and/or defogging. Accordingly, such factors will determine the usage and number of channels 630 as well as the construction, size, shape and configuration of the adapter ring 302 of additional embodiments of the view optimizer 200.

As shown in FIG. 5A, a laparoscope opening 622 is defined within the inner rim 620 of the adapter ring. The laparoscope opening 622 is adapted to receive the laparoscope 100 and allow for the laparoscope 100 to enter the guard tube 304. The laparoscope opening 622 may be any size, shape or configuration that allows for the receipt of the laparoscope 100.

Referring now to FIG. 5B, a rear perspective view of the adapter ring 302 is shown. As shown in FIG. 5B, the laparoscope opening 622 extends through the adapter ring 302. Also as shown in FIG. 5B, the channels 630 defined within the adapter ring 302 extend to the rear of the adapter ring 302 and open into arcuate shaped openings 640, 642, 644 and 646 defined within the rear surface of the adapter ring 302. As can be seen in FIG. 5B, two of the channels 630 connect with opening 640, one channel 630 connects with opening 642, two of the channels 630 connect with opening 644 and one of the channels 630 connects with opening 646. In this manner, one pair of the channels 630 are jointly connected to opening 640 and one pair of the channels are jointly connected to opening 644. Accordingly, the gas and/or liquid traveling through such channels 630 will jointly flow through openings 640 and 644. Also, any gas and/or liquid which enters openings 640 or 644, will flow into the pair of channels 630 connected with opening 640 or 644. Consequently, this allows for one source of gas and/or liquid to be divided into the flow of gas and/or liquid through a pair of channels 630 of the adapter ring and, consequently, a pair of channels 512 of the guard tube 304.

In the illustrated embodiment of the view optimizer 200, opening 640 is adapted to receive gas for delivery to the objective lens of the laparoscope 100 through the lens guard 210, opening 642 is adapted to receive liquid for delivery to the objective lens of the laparoscope 100 through the lens guard 210, and opening 644 is adapted for the passage of the exhaust gases leaving the patient's body cavity via exhaust vents 516 and passing through the lens guard 210. In the illustrated embodiment of the view optimizer 200, opening 646 is not operable to receive the flow of either gas or liquid, however in additional embodiments of the view optimizer 200, opening 646 may be functional. As mentioned previously, various additional embodiments of the view optimizer 200 may utilize both gas and liquid or one of gas or liquid for delivery to the objective lens of the laparoscope for cleaning and/or defogging. In addition, additional embodiments of the view optimizer may not include a controlled leak function. Accordingly, such factors will affect the construction, size, shape, configuration and functionality of the adapter ring 302, the channels 630 of the adapter ring 302, and the openings 640, 642, 644, and 646 of the adapter ring 302 of additional embodiments of the view optimizer 200.

Referring again to FIG. 3, the view optimizer 200 includes a connection plate 310 that is adapted to abut the adapter ring 302. The connection plate 310 of the illustrated embodiment is a generally planar, circular disc with a central opening 311 defined through it, and is adapted to permit the laparoscope 100 to pass through the connection plate 310. The connection plate 310 also has four openings 312 defined through it radially outward from the central opening 311. The openings 312 are adapted to receive fluid connectors 315. While the connection plate 310 of the illustrated embodiment has four fluid

connectors 315, additional embodiments of the connection plate 310 may have any number of fluid connectors 315. The connection plate 310 is adapted to abut against the adapter ring 302 and seal against the openings 640, 642, 644 and 646. Each of the four fluid connectors 315 mounted within the connection plate 310 coincides with one of the openings 640, 642, 644 and 646 of the adapter ring 302 described in connection with FIG. 5. Thus, fluid flowing through one of the fluid connectors 315 is free to pass through the connection plate 310 into one of the openings 640, 642, 644 and 646 of the adapter ring, through the channels 630 of the adapter ring, through one of the channels 512 of the guard tube, through one of the channels of the exhaust ring and through the end ring 308 for delivery to the objective lens. In addition, exhaust gas that enters the exhaust vents 516 may pass up the guard tube 304, through the adapter ring 302 and into one of the fluid connectors 315. Additional embodiments of the view optimizer may not include a connector plate 310 or fluid connectors 315.

Referring again to FIG. 5B, projecting outwardly from the adapter ring 302 are three fastener portions 650, each fastener portion 640 having a fastener opening defined therethrough. As shown in FIG. 6, the fastener portions 650 are utilized to mount the adapter ring 302 and, consequently, the lens guard 210 to the flow controller 220. Additional embodiments of the sheath assembly 200 may have any number of fastener portions 650. The adapter ring 302 of the illustrated embodiment is attached to the flow controller 220 with conventional screws, however, other suitable fasteners, such as adhesives, rivets, tab and slots, etc. could also be used. When the adapter ring 302 and lens guard 210 are mounted to the flow controller 220, the fluid connectors 315 project into the interior of the flow controller 220. Also, as mentioned previously, the lens guard 210 and the flow controller 220 may be formed as a one-piece construction in additional embodiments of the view optimizer 200 or may be located remotely from one another and not directly connected to one another. As a result, all embodiments of the view optimizer 200 may not include an adapter ring 302. It should be understood that additional embodiments of the view optimizer 200 may utilize various methods for mounting the lens guard 210 to the flow controller 220.

Referring again to FIG. 3, the flow controller 220 will be described with more particularity. The flow controller 220 of the illustrated embodiment of the view optimizer 200 generally includes a base portion 318, a handle portion 320 and an end cap 330. The base portion 318, handle portion 320 and end cap 330 of the illustrated embodiment are adapted to surround and enclose other portions of the view optimizer 200. The base portion 318, handle portion 320 and end cap 330 of the illustrated embodiment are molded from plastic, however, other suitable materials can also be used. It should be understood that the base portion 318, handle portion 320 and end cap 330 of the view optimizer 200 are not limited to the size, shape or configuration set forth in FIG. 3. The base portion 318, handle portion 320 and end cap 330 of the flow controller 220 of the view optimizer 200 can have any size, shape or configuration that can support and/or enclose other components of the view optimizer 200.

The base portion 318, handle portion 320 and end cap 330 are fastened together with a plurality of fasteners 332. The fasteners 332 of the illustrated embodiment are conventional screws, however, it should be understood that any suitable attachment means could be used. Examples of additional fasteners that can be used include, but are not limited to, any type of screws or bolts, anchors, rivets, cotter pins, clips, snaps, straps, ties, adhesives, weldments, etc. In addition, it

should be understood that the flow controller 220 could be formed as one unitary piece in additional embodiments, and need not be provided as multiple pieces that are assembled together.

The base portion 318 of the flow controller 220 has an outer wall 334 that defines an interior cavity 336. The configuration of the interior cavity 336 of the base portion 318 is adapted to support and enclose other components of the view optimizer 200. A scope receiver portion 338 extends from the outer wall 334 of the base portion 318 and opens into the interior cavity 336 of the base portion 318. The scope receiver portion 338 is adapted to receive the laparoscope 100. The scope receiver portion 338 of the illustrated embodiment of the view optimizer is a cylindrically shaped, threaded channel. However, the scope receiver portion 338 is not limited to this shape or configuration and can have any shape or configuration that allows it to receive the laparoscope 100. The scope receiver portion 338 of the illustrated embodiment is adapted to receive a grommet 340 that has a cylindrical shape with a opening defined therethrough. The grommet 340 of the illustrated embodiment is rubber, however other suitable materials may also be used, such as plastic or a composite material. The threads of the scope receiver portion 338 are adapted to mate with the threads of a nut 342 which can be tightened onto the scope receiver portion 338. The nut 342 of the illustrated embodiment has an opening defined through it. A second opening (not shown in the figures) is defined within the bottom wall of the base portion 318 of the flow controller 220. This second opening is in communication with the lens guard 210 that is connected to the base portion 318 of the main body (as shown in FIG. 6).

When the view optimizer 200 is in use, the distal end 120 of the main body 110 of a laparoscope 100 is inserted, in turn, through the opening defined within the nut 342, the opening defined within the grommet 340, and the opening defined within the scope receiver portion 338 by the scope operator. The main body 100 of the laparoscope 100 is then passed through the scope receiver portion 338 and through the base portion 318 of the flow controller 220 into the lens guard 210. Once the distal end 120 of the laparoscope 100 reaches the desired position within the lens guard 210, the nut 342 can be tightened down onto the threads of the scope receiver portion 338. This tightening of the nut 342 forces the grommet 340 to be wedged between the surface of the scope receiver portion 338 and the laparoscope 100, thereby locating the laparoscope in the desired position relative to the flow controller 220 and the lens guard 210, and preventing both linear and rotational movement of the laparoscope relative to the flow controller 220 and the lens guard 210. However, one or both of linear or rotational movement may be allowed in alternative embodiments.

As illustrated in FIG. 3, the handle portion 320 of the flow controller 220 has a main wall 350 that defines a partially enclosed space. The configuration of the handle portion 320 is adapted to support and enclose other components of the view optimizer 200. The partially enclosed space of the handle portion 320 abuts with the interior cavity 336 of the base portion 318 so the partially enclosed space of the handle portion 320 and the interior cavity 336 of the base portion 318 are in communication when the base portion 318 and the handle portion 320 are joined. Referring to the illustrated embodiment of FIG. 3, a burst actuator compartment 352 and a gas/liquid actuator compartment 354 are defined within the main wall 350 of the handle portion 320. The burst actuator compartment 352 is adapted to hold the burst actuator 360 and the gas/liquid actuator compartment 354 is adapted to hold the gas/liquid actuator/regulator 250. The burst actuator com-

partment 352 and the gas/liquid actuator compartment 354 of the handle portion 320 are in communication with each other as well as being in communication with the interior cavity 336 of the base portion 318.

The handle portion 320 of the illustrated embodiment of the view optimizer includes an end cap 330 that is removably attached to the handle portion 320 of the flow controller 220. The end cap 330 is adapted to fully enclose the gas/liquid actuator compartment 354 of the handle portion 320. Additional embodiments of the view optimizer 200 are provided without such an end cap 330. As mentioned previously, additional embodiments of the view optimizer may include a one-piece flow controller 220 as opposed to the multi-piece flow controller 220 of the illustrated embodiment. The main body can have any shape or configuration that allows it to support and/or enclose other portions of the view optimizer 200.

The gas inlet 230 and the fluid inlet 240 of the flow controller 220 extend into the gas/liquid actuator compartment 354 of the handle portion 320 of the flow controller 220. The gas inlet 230 and the liquid inlet 240 of the illustrated embodiment of the view optimizer 200 are cylindrical tubes extending outwardly from the surface of the flow controller 220. The gas inlet 230 and liquid inlet 240 are formed from plastic, but a variety of suitable materials could also be used. It should be mentioned that additional shapes and configurations could be used for the gas inlet 230 and liquid inlet 240. The gas inlet 230 and the fluid inlet 240 of the flow controller 220 receive gas and liquid respectively from external sources. The gas inlet 230 and liquid inlet 240 can have any shape or configuration that allows for the connection of the view optimizer 200 to external gas and liquid sources.

It should be understood that additional embodiments of the view optimizer 200 may include gas and/or liquid sources that are located internally within the view optimizer 200 itself, thus eliminating the need for a means of connecting the view optimizer 200 to external sources of gas and/or liquid. In addition, it should also be understood that additional embodiments of the view optimizer utilize only gas or only liquid. Whether or not the view optimizer 200 utilizes gas, liquid, or both will determine whether a gas or liquid inlet is provided with various additional embodiments of the view optimizer 200.

The gas/liquid actuator/regulator 250 of the illustrated embodiment of the view optimizer is housed within the gas/liquid actuator compartment 354 of the handle portion 320 of the flow controller 220. The gas/liquid actuator/regulator 250 of the view optimizer 200 can be formed of one of a variety of actuation means. The gas/liquid actuator/regulator 250 of the illustrated embodiment of the view optimizer 200 is a control valve, namely, a manually controlled switching valve. It should be understood, however, that additional embodiments of the view optimizer 200 may include a variety of different types of gas/liquid actuator. Additional embodiments of the view optimizer 200 may include a variety of manually or electrically controlled valves or other device. The gas/liquid actuator/regulator 250 may be any valve or similar device that actuates and/or regulates the flow of the gas and/or liquid utilized by the view optimizer 200 for delivery to the objective lens of the laparoscope 100. The gas/liquid actuator/regulator 250 of the illustrated embodiment is formed from plastic; however, other suitable materials including metals and composites may also be used.

The gas/liquid actuator/regulator 250 of the embodiment of the view optimizer 200 illustrated in FIG. 3 includes a gas inlet 358, a liquid inlet 360, a gas outlet 362 and a liquid outlet 364. Referring to FIG. 4, the gas inlet 230 of the flow controller

troller 220 is connected to the gas inlet 358 of the gas/liquid actuator/regulator 250 and the liquid inlet 240 is connected to the liquid inlet 360. The embodiment of the gas/liquid actuator/regulator 250 illustrated in FIG. 3 includes an actuation switch 366. The actuation switch 366 of the illustrated embodiment is a push-button that can be selectively operated to actuate the gas/liquid actuator/regulator 250. However, it should be understood that a variety of different switches or other actuation devices can be utilized to perform this function, and the view optimizer 200 of this application is not limited to a push-button type switch. The actuation switch 366 can be any type of switch or actuation device that can serve to actuate the gas/liquid actuator.

The gas/liquid actuator/regulator 250 of the illustrated embodiment of the view optimizer 200 is operable to switch between two states, a gas flow state and a liquid flow state. In the gas flow state, gas from an external gas source, such as an insufflator in the case of the illustrated embodiment, flows through the gas inlet 230 of the flow controller 220, through the gas inlet 358 of the gas/liquid actuator/regulator 250, through the gas/liquid actuator/regulator 250 and out the gas outlet 362 of the gas/liquid actuator/regulator 250. When the gas/liquid actuator/regulator 250 is in the gas flow state, liquid is prevented from flowing through the gas/liquid actuator/regulator 250 and out of the liquid outlet 364. Conversely, when the gas/liquid actuator/regulator 250 is in the liquid flow state, liquid from an external source flows through the liquid inlet 240 of the flow controller 220, through the liquid inlet 360 of the gas/liquid actuator/regulator 250, through the gas/liquid actuator/regulator 250 and out the liquid outlet 364 of the gas/liquid actuator/regulator 250. When the gas/liquid actuator/regulator 250 is in the liquid flow state, gas is prevented from flowing through the gas/liquid actuator/regulator 250 and out of the gas outlet 362.

The gas/liquid actuator/regulator 250 of the illustrated embodiment is biased towards the gas flow state and delivers a generally continuous flow of gas when in the gas flow state. In this manner, the view optimizer 200 of the illustrated embodiment delivers a generally continuous flow of gas to the objective lens of the laparoscope 100 when the gas/liquid actuator/regulator 250 is in the gas flow state. The gas/liquid actuator/regulator 250 of the illustrated embodiment remains in the gas flow state with the view optimizer delivering a generally continuous flow of gas to the objective lens of the laparoscope until an operator switches the gas/liquid actuator/regulator 250 to the liquid flow state by pressing the actuation switch 366 of the gas/liquid actuator/regulator 250. When the gas/liquid actuator/regulator 250 of the illustrated embodiment is switched to the liquid flow state, gas is not permitted to flow through the gas/liquid actuator/regulator 250. The gas/liquid actuator/regulator 250 of the illustrated embodiment only remains in the liquid flow state for as long as the operator is holding the actuation switch 366. Once the operator releases the actuation switch 366, the gas/liquid actuator of the illustrated embodiment returns to the gas flow state. Additional embodiments of the gas actuator/regulator 250 could remain in the liquid flow state until an operator presses on the actuation switch 366. In additional embodiments of the view optimizer, the actuation switch 250 may allow for the flow of both liquid and gas simultaneously. In yet additional embodiments, the gas/liquid actuator/regulator 250 may be biased towards the liquid flow state. Additionally, some view optimizers contemplated by this detailed description may only utilize gas or liquid and the actuation switch 366 of such embodiments will only activate or deactivate the flow of gas or liquid not both and not switch between the flow of gas or liquid. And in still other embodiments, the appara-

tuses may include more than one actuation switch, each of which independently activates and deactivates the flow of a liquid or a gas, or combinations thereof.

The burst actuator/regulator 260 of the illustrated embodiment of the view optimizer 200 is housed within the burst actuator compartment 352 of the handle portion 320 of the flow controller 220. The burst actuator/regulator 260 of the view optimizer 200 can be formed of one of a variety of actuation means. As shown in FIG. 3, the burst actuator/regulator 260 of the embodiment of the view optimizer 200 illustrated in FIG. 3 is a manually operated, pneumatic bulb. However, it should be understood that the burst actuator/regulator 260 can be a variety of different manually or electrically operated devices. The burst actuator/regulator 260 can be any device that allows for the actuation and/or regulation of the burst function of the view optimizer 200. The burst actuator/regulator 260 of the illustrated embodiment is formed from rubber, however other suitable materials may be used. The burst actuator/regulator 260 of the illustrated embodiment has an inlet 370 and an outlet 372. The burst actuator/regulator 260 of the illustrated embodiment is adapted to deliver a burst or bolus of gas and/or liquid to the objective lens of the laparoscope 100 when activated by an operator. It will be understood that in various other embodiments, the apparatuses may include more than one burst actuator, each of which is adapted to work independently to deliver a burst or bolus of a liquid or a gas, or combinations thereof.

The burst actuator/regulator 260 of the additional embodiments of the view optimizer 200 may be adapted to serve as a gas accumulator (not shown) that accumulate pressurized gas from the insufflator, or from one or more other or additional gas sources. In the event that the insufflator cycles into the static, non insufflating state, the gas within the gas accumulator of such additional embodiments is delivered to the objective lens of the laparoscope via the view optimizer 200. This delivery of gas from the gas accumulator ensures that the view optimizer 200 is supplied with a generally steady supply of gas even when the insufflator cycles into the static state. In this manner, the gas accumulator would act as a damping mechanism to smooth out the cyclic on/off of the insufflator and ensure that a generally steady, continuous flow of gas is delivered to the objective lens of the laparoscope 100.

As an example, the burst actuator/regulator 260 of some additional embodiments may be an elastic, compliant chamber that expands to accumulate gas from the insufflator. In this manner, the burst actuator/regulator 260 could be used to actuate the delivery of a burst or bolus of gas and/or liquid to the objective lens as well as serving as a gas accumulator. A backflow valve may be provided with such burst actuators 260 of additional embodiments to prevent gas from returning to the insufflator from the burst actuator/regulator 260. Such gas accumulators are adapted to accumulate gas from the insufflator until a predetermined, threshold pressure of gas within the gas accumulator is reached. Once the threshold pressure is reached, the gas accumulator would not accumulate any additional gas from the insufflator. This threshold pressure could be maintained within the accumulator either by the use of a valve or similar control mechanism or simply be maintained by the pressure of the flow of gas supplied by the insufflator.

The gas accumulator of such embodiments is adapted to maintain a pressure that is equal to or greater than the predetermined pressure at which the patient's body cavity is desired to be maintained. Once the pressure within the patient's body cavity drops below the predetermined pressure, due to the cycling off of the insufflator or some other

reason, the gas accumulator would deliver gas to the objective lens of the laparoscope 100, thereby, also delivering gas to the patient's body cavity. In instances where an elastic, compliant chamber is supplied as the gas accumulator, the chamber will elastically contract in response to a pressure differential between the gas accumulator and the patient's body cavity. This contraction of the gas accumulator would serve to deliver gas to the objective lens of the laparoscope 100 and the patient's body cavity. The delivery of gas by such a gas accumulator could be controlled by the utilization of a valve or similar control mechanism. The delivery of such gas could also be delivered in a manner that is not capable of being controlled by the user.

It should be understood that the gas accumulator described above could be provided as a single chamber or multiple chambers. The gas accumulator could be incorporated with the burst actuator/regulator 260 as described above or could be provided separately from the burst actuator/regulator 260. In embodiments in which the burst actuator/regulator 260 and the accumulator function are provided separately from one another, they could each be connected to the insufflator in series or in parallel with respect to one another. Once all or a portion of the gas contained within the gas accumulator has been delivered to the objective lens of the laparoscope, the gas accumulator must be refilled with gas. If the gas accumulator is connected in series with the burst actuator/regulator 260, or other component of the view optimizer 200 that delivers gas to the objective lens, all or a portion of the flow of gas from the insufflator will first fill the gas accumulator to capacity prior to being delivered to the objective lens of the laparoscope. Due to this phenomenon, a decreased amount of flow will be delivered to the objective lens during the filling of the gas accumulator. Upon the initial startup of the insufflator or the cycling of the insufflator to an insufflation state from a static state, this can result in a time period during which little or no gas is delivered to the objective lens of the laparoscope during the filling of the gas accumulator. To prevent this from occurring, in some embodiments of the view optimizer, the gas accumulator is connected to the insufflator in parallel with relation to the burst actuator/regulator 260 or other components of the view optimizer 200 that deliver gas to the objective lens of the laparoscope to ensure that an effective flow of gas to the objective lens is maintained while the gas accumulator is being filled. In such embodiments, a portion of the gas from the insufflator can be diverted to refill the accumulator only if this diverted flow will not cause the flow of gas that is being delivered to the objective lens to drop below an effective amount. In various embodiments, the flow being diverted to the accumulator can be controlled by a valve or other similar control means.

It should be understood that the gas accumulator of additional embodiments could be adapted to accommodate a variety of different volumes of pressurized gas. In yet additional embodiments, the gas accumulator could be a non-compliant chamber that is activated by a control switch or other actuation means to deliver gas to the objective lens of the laparoscope 100 when the insufflator ceases insufflating. Such a gas accumulator could be electronically controlled and connected to the insufflator via electronic circuitry so as to be responsive to the cycling of the insufflator. Finally, it should be understood that additional embodiments of the view optimizer 200 may not be supplied with gas from an insufflator, but, rather, may include a gas supplying device incorporated within the view optimizer 200 that is comparable to the insufflator.

Referring again to FIG. 3, the gas outlet 362 of the gas/liquid actuator/regulator 250 of the illustrated embodiment of the view optimizer 200 is connected to the inlet 370 of the

burst actuator/regulator 260. In the embodiment of the view optimizer 200 illustrated in FIG. 4, the gas/liquid actuator/regulator 250 is connected directly to the inlet 370 of the burst actuator/regulator 260. In other embodiments of the view optimizer 200, the gas/liquid actuator/regulator 250 and the burst actuator/regulator 260 are connected indirectly with other intermediate parts being located between them, such as tubing or conduit. In addition, it should be understood that the gas/liquid actuator/regulator 250 and the burst actuator/regulator 260 need not be connected with one another in all embodiments of the view optimizer 200, as they may each receive gas and/or liquid from separate sources. Finally, it should be understood that all embodiments of the view optimizer 200 contemplated by this detailed description do not include both a gas/liquid actuator/regulator 250 and a burst actuator, as additional embodiments may be provided with only a gas/liquid actuator/regulator 250 or burst actuator/regulator 260.

The liquid outlet 364 of the gas/liquid actuator/regulator 250 is connected to one of the fluid connectors 313 of the connection plate by tubing (not shown) that travels through the internal cavity defined within the handle portion 220 and base portion 318 of the flow controller 220. Similarly, the outlet 372 of the burst actuator/regulator 260 is connected to one of the fluid connectors 313 of the connection plate 310 by tubing (not shown) which travels through the internal cavity defined within the handle portion 220 and base portion 318 of the flow controller 220. While tubing is used in some embodiments of the sheath assembly, other suitable methods could be used, such as any type of piping or conduit or flow channels defined within portions of the flow controller 220. The view optimizer of this detailed description is not limited with respect to the method which is used to connect the gas and/or liquid source to the lens guard 210 for delivery to the objective lens of the laparoscope 100.

When the gas/liquid actuator/regulator 250 is in the gas flow state, gas flows from the gas source into the gas inlet 230 of the flow controller 220, through the gas/liquid actuator/regulator 250, through the burst actuator/regulator 260, through a piece or series of tubing into a fluid connector 313 of the connector plate 310, through opening 640 of the adapter ring 302, through a pair of channels 630 of the adapter ring 302, through a pair of corresponding channels 512 of the guard tube 304, through channels 520, 521 of the exhaust ring 306, and is directed across the lens of the laparoscope 100 by passageways 528, 530 of the end ring 308. As mentioned previously, the gas/liquid actuator/regulator 250 of the illustrated embodiment is biased towards the gas flow state and delivers a generally continuous flow of gas from the insufflator when in this state. Accordingly, when the view optimizer 200 of the illustrated embodiment is in the normal operation state, a generally continuous flow of gas is directed across the face of the objective lens of the laparoscope 100 through passageways 528, 530 of the end ring 308. As set forth above, this gas flows in a path that is generally parallel to the objective lens of the laparoscope.

This generally continuous flow of gas across the face of the objective lens of the laparoscope 100 serves to prevent the objective lens from fogging, particularly under circumstances when there is a significant temperature and/or humidity differential between the operating room environment and the body cavity of the patient. The generally continuous flow of gas across the objective lens of the laparoscope also serves to deflect away from the objective lens any blood, bodily fluids, pieces of tissue, fat or other bodily material that may be encountered by the objective lens of the laparoscope 100 during an operative procedure. If blood, bodily fluids, pieces

of tissue, fat or other bodily material is contacted by and sticks to the objective lens of the laparoscope 100, the gas flow from passageways 528, 530 serves to remove the material from the objective lens of the laparoscope 100 and to prevent the material from obstructing the view of the surgeon or medical technician through the scope.

The view optimizer 200 of the illustrated embodiment is adapted for use with conventional insufflators that typically provide gas at a flow rate of between zero (0) and fifteen (15) liters per minute when cycling during normal operation. Of course, other insufflators may deliver gas at flow rates that are considerably higher or lower, and may still be useful with the view optimizers disclosed herein. Thus, the view optimizer 200 of this detailed description can be adapted to be used with insufflators having a variety of flow rates. When in the gas flow state during normal operation, the view optimizer 200 of the illustrated embodiment is adapted to divert approximately 9% to 18% of this gas provided from the insufflator for delivery to the objective lens of the laparoscope 100 through the lens guard 210. Accordingly, the remainder of the gas provided by the insufflator continues to be delivered to the patient's body cavity through one or more of the trocars and not pass through the view optimizer 200. For example, if the insufflator produces 1 liter per minute (L/min), then 0.1 L/min (10%) would go through the view optimizer 200 to the patient and 0.9 L/min would go through the insufflator trocar to the patient. Additional embodiments of the view optimizer 200 may divert more or less of the flow from the insufflator to the view optimizer 200. Accordingly, in various embodiments, the view optimizer 200 may divert about 8, 9, 10, 11, 12, 13, 14, 15, 16, 17, or 18% of the gas provided from the insufflator. However it should be understood that additional embodiments of the view optimizer 200 may divert gas from the insufflator in excess of 19, 20, 25, 30, 40, 50, 60, 70, 80, 90% or more. And it will be appreciated that in yet other embodiments, the source of the gas may be from other than the insufflator, in which case there is no diversion of gas from direct delivery to the patient's body cavity.

When in the gas flow state during normal operation, the view optimizer 200 of the illustrated embodiment delivers a generally continuous flow of gas across the objective lens of the laparoscope 100 at a flow rate between zero (0) and ten (10) liters per minute. In some embodiments, the view optimizer 200 delivers a flow of gas at a flow rate between 0.01 and five (5) liters per minute, and in yet other embodiments the view optimizer 200 delivers a flow of gas at a flow rate between two and a half (2.5) and five (5) liters per minute. This generally continuous flow of gas across the objective lens of the laparoscope 100 forms a gas "screen," or "shield." This gas "screen" or "shield" of continuous gas flow across the objective lens of the laparoscope 100 is delivered at a velocity of between zero (0) and about forty (40) meters per second. In some embodiments, the velocity of gas is from about nineteen (19) to thirty eight (38) meters per second. Accordingly, in various embodiments, the flow rate of the gas across the lens is about 0, 0.01, 0.02, 0.03, 0.04, 0.05, 0.06, 0.07, 0.08, 0.09, 0.1, 0.2, 0.3, 0.4, 0.5, 0.6, 0.7, 0.8, 0.9, 1.0, 1.1, 1.2, 1.3, 1.4, 1.5, 1.6, 1.7, 1.8, 1.9, 2.0, 2.1, 2.2, 2.3, 2.4, 2.5, 3, 4, 5, 6, 7, 8, 9 or 10 L/min, or increments thereof. And the velocity of the gas screen is about 1, 2, 3, 4, 5, 6, 7, 8, 9, 10, 11, 12, 13, 14, 15, 16, 17, 18, 19, 20, 21, 22, 23, 24, or 25 m/s. However it should be understood that additional embodiments of the view optimizer 200 may deliver gas to the objective lens of the laparoscope at a variety of different flow rates and velocities, in which case such flow rates may exceed 10 L/min or greater and the velocities may exceed 25, 30, 40, 50, 60, 70, 80, 90 or 100 m/s or greater.

During a surgical procedure, blood, bodily fluids, pieces of tissue, fat or other bodily material may become lodged upon the objective lens of the laparoscope and effectively resist deflection or removal by the gas flow provided by the view optimizer in normal operation state. To help facilitate the removal of such adherent material, the view optimizer 200 of the illustrated embodiment provides a burst flow feature. An operator may activate the burst flow feature of the illustrated embodiment of the view optimizer 200 through the use of the burst actuator/regulator 260. As mentioned previously, the burst actuator/regulator 260 of the illustrated embodiment is a manually operated, pneumatic bulb. To activate the burst flow feature of the illustrated embodiment of the view optimizer 200, an operator squeezed the pneumatic bulb of the burst actuator/regulator 260. When the burst actuator/regulator 260 is activated, the view optimizer 200 of the illustrated embodiment delivers a burst or bolus of gas from the insufflator to the objective lens of the laparoscope 100. During the burst flow state, the view optimizer 200 of the illustrated embodiment delivers a burst or bolus of gas at a flow rate between zero (0) and twenty (20) liters per minute at a velocity of between zero (0) and one hundred and forty five (145) meters per second. Accordingly, in various embodiments, the gas burst flow rate of the gas across the lens is about 0, 1, 2, 3, 4, 5, 6, 7, 8, 9, 10, 11, 12, 13, 14, 15, 16, 17, 18, 19, and 20 L/min, or increments thereof. And the velocity of the gas burst flow is about 1, 2, 3, 4, 5, 6, 7, 8, 9, 10, 11, 12, 13, 14, 15, 16, 17, 18, 19, 20, 25, 30, 35, 40, 45, 50, 55, 60, 65, 70, 75, 80, 85, 90, 95, 100, 115, 130, or 145 m/s, or increments thereof. However it should be understood that additional embodiments of the view optimizer 200 may deliver gas burst flow to the objective lens of the laparoscope at a variety of different flow rates and velocities, in which case such flow rates may exceed 20, 25, 30, 35, 40, 45, 50 L/min or greater and such velocities may exceed 150, 155, 160, 165, 170 m/s or greater. The burst or bolus of gas serves to remove blood, bodily fluids, pieces of tissue, fat or other bodily material lodged upon the objective lens of the laparoscope that is resistant to the gas flow provided by the view optimizer in the normal operation state.

As mentioned previously, when the gas/liquid actuator/regulator 250 of the view optimizer 200 of the illustrated embodiment is in the liquid flow state, liquid is delivered to the objective lens of the laparoscope 100 and the delivery of gas ceases. When the gas/liquid actuator/regulator 250 is in the liquid flow state, liquid flows from the liquid source into the liquid inlet 240 of the flow controller 220, through the gas/liquid actuator/regulator 250, through a piece or series of tubing into a fluid connector 313 of the connector plate 310, through opening 642 of the adapter ring 302, through a channel 630 of the adapter ring 302, through a corresponding channel 512 of the guard tube 304, through channel 518 of the exhaust ring 306, and is directed across the lens of the laparoscope 100 by passageway 526 of the end ring 308. Accordingly, when the view optimizer 200 of the illustrated embodiment is in the liquid flow state, a generally continuous flow of liquid is directed across the face of the objective lens of the laparoscope 100 through passageway 526 in a path that is generally parallel to the objective lens. As shown in FIG. 4C, the passageway 526 of the end ring 308 that delivers the fluid to the objective lens is located in a position which directs the flow of the liquid in a path which is generally perpendicular to the flow of the gas provided by channels 528, 530 of the end ring 308. However, it should be understood that the view optimizer 200 of the illustrated embodiment is not limited to this configuration of the flow of liquid and gas and additional embodiments of the view optimizer 200 may provide a dif-

ferent configuration of gas and/or liquid flow. In addition, the gas and/or liquid flow of additional embodiments of the view optimizer may be angled towards or away from the objective lens of the laparoscope 100.

When the gas/liquid actuator is in the liquid flow state, the view optimizer 200 of the illustrated embodiment delivers liquid at a volume of generally between zero (0) and 0.4 liters per minute at a velocity of generally between zero (0) to 0.0075 meters per second. However, it should be understood that additional embodiments of the view optimizer 200 may deliver liquid at various other flow rate and velocities. Accordingly, in various embodiments, the flow rate of the liquid across the lens is about 0, 0.1, 0.2, 0.3, or 0.4 L/min. And the velocity of the liquid flow is about 0 to about 0.0075 m/s. However it should be understood that additional embodiments of the view optimizer 200 may deliver liquid to the objective lens of the laparoscope at a variety of different flow rates and velocities, in which case such flow rates may exceed 0.4, 0.5, 0.6, 0.7, 0.8, 0.9, 1.0 or greater and such velocities may exceed 0.0075 m/s or greater. This delivery of liquid to the objective lens of the laparoscope 100 serves to defog or clean the objective lens.

As the illustrated embodiment of the view optimizer 200 is adapted to deliver a generally continuous flow of gas to the objective lens of the laparoscope 100, this cycling of the insufflator needs to be prevented. For this reason, the view optimizer 200 of the illustrated embodiment is provided with exhaust vents 516 located within the exhaust ring 306. When the laparoscope 100 and the view optimizer 200 are inserted into a patient's abdominal cavity during a surgical procedure, the exhaust vents 516 of the exhaust ring 306 are located within the patient's abdominal cavity. Insufflated gas present in the patient's abdominal cavity is able to enter the exhaust vents 516 and travel through a pair of the channels 512 of the guard tube 304, thus exiting the patient's abdominal cavity. Due to the pressure differential between the interior of the lens guard 210 and the patient's abdominal cavity, this exhaust gas travels through the channels 512 of the guard tube 304, through a pair of the channels 630 of the adapter ring 302, through opening 644 of the adapter ring and through one of the fluid connectors 313 located in the connection plate 310. The fluid connector 313 which the exhaust gas travels through projects into the base portion 318 of the flow controller 220.

As shown in FIG. 6, an exhaust valve 710 is mounted within the base portion 318 of the flow controller 220. The fluid connector 313 through which the exhaust gas from within the patient's abdominal cavity passes is connected to the exhaust valve 710 by a piece of or series of tubing (not shown). The exhaust valve 710 can be a variety of different valves or similar devices. The exhaust valve 710 can be any device that can be used to control the flow of the exhaust gases traveling through the view optimizer 200. The exhaust valve 710 is in communication with exhaust vent 720 defined within the base portion 318 of the flow controller 220, which is adapted to allow the exhaust gas to exit the view optimizer to the surroundings. The exhaust valve 710 is operable to adjust the flow rate of the exhaust gas exiting the view optimizer 200 via exhaust vent 720. The controlled leak created by gas entering the lens guard 210 via the exhaust vents 516 and exiting the view optimizer via exhaust vent 720 into the surroundings helps to ensure that the pressure within the patient's abdominal cavity remains below the pre-determined pressure that the insufflator is set to maintain the patient's abdominal cavity. This ensures that the insufflator will continuously insufflate the patient's abdominal cavity and will not shut off during a surgical procedure. Due to the fact that

the insufflator is prevented from shutting off, the view optimizer 200 of the illustrated embodiment will be supplied with a generally continuous supply of gas for delivery to the objective lens of the laparoscope. The flow rate of the gas exiting the patients abdominal cavity via exhaust vents 516 can be controlled via exhaust valve 710 to allow for the scope operator to create a desired amount of leakage from the patient's abdominal cavity, while not compromising the effectiveness of the insufflation. As stated previously, however, it should be understood that additional embodiments of the view optimizer 200 may not provide a controlled leak function and, thus, may not include exhaust vents 516, an exhaust ring 306, exhaust valve 710 or exhaust valve 720. In addition, the view optimizer of this detailed description is not limited to the configuration set forth above with respect to the exhaust of gases from within the patients abdominal cavity through the view optimizer, as additional embodiments of the view optimizer may include exhaust systems that are constructed differently.

The illustrated embodiment of the view optimizer 200 is adapted to deliver a generally continuous flow of gas to the objective lens of a laparoscope 100 via end ring 308 of the lens guard 210 for the cleaning and/or defogging of the lens and to deliver a flow of liquid to the objective lens of the laparoscope 100 when the operator desires. It should be understood that additional embodiments of the view optimizer 200 may be adapted to deliver a generally continuous flow of only liquid to the objective lens of the laparoscope 200 or both liquid and gas simultaneously. In addition, additional embodiments of the view optimizer 200 may be adapted to not deliver a continuous flow of gas and/or liquid but, rather, be adapted to only deliver a flow of gas and/or liquid upon the activation of an actuation device.

The illustrated embodiment of the view optimizer 200 is also adapted to deliver a burst or bolus of gas to the objective lens of the laparoscope upon the activation of a burst actuator/regulator 260. It should be understood that additional embodiments of the view optimizer may be adapted to deliver a burst or bolus of liquid to the objective lens of the laparoscope 200. It should also be understood that additional embodiments of the view optimizer may be provided without this burst function.

Finally, the illustrated embodiment of the view optimizer 200 is adapted to create a controlled leak of the gases from within the patients abdominal cavity to ensure that the insufflator does not turn off during a surgical procedure or to diminish the frequency of such stoppages of the insufflator. It should be understood that all embodiments of the view optimizer do not include such a controlled leak function. In addition, yet additional embodiments of the view optimizer 200 may create a steady leak, which is not controllable by the operator.

According to some embodiments, vibration of the objective lens of the laparoscope is utilized as an additional means for removing moisture and debris from the objective lens and/or preventing moisture and debris from adhering to the objective lens. According to some such embodiments, the view optimizer 200 is adapted to utilize the flow of gas from the insufflator to vibrate the objective lens. For example, the end ring 308 is structured in such embodiments in such a way that the flow of gas over or through the end ring 308 vibrates the end ring 308 and, thus, vibrate the objective lens as well. One such embodiment includes an end ring 308 including flexible flaps that are adapted to vibrate the end ring 308 as gas from the insufflator flows over the flaps. Additional embodiments of the view optimizer 200 include mechanical means for vibrating the objective lens that do not utilize the flow of

gas from the insufflator. For example, some embodiments utilize a piezoelectric end ring 308 or one or more eccentric weights to vibrate the objective lens. It should be understood that in additional embodiments of the view optimizer 200, vibration of the objective lens may be provided in combination with one or more of the cleaning and/or defogging methods previously described or may be provided alone.

EXAMPLES

Example 1

Effect of Venting and Incidence of Scope Removal

Evaluation of effect of venting on insufflator function was evaluated during a laparoscopic surgical procedure. The ambient surgical room temperature was 67°F, the temperature of the carbon dioxide supply was 60 F, and the room humidity was 74%. The following general observations of insufflator function were recorded: after establishing constant pressure in the abdomen sufficient to shut off insufflator operation, followed by a sudden pressure drop in the surgical cavity, there was a 2-3 sec lag before the insufflator restarted. During the standard laparoscopic procedure, the insufflator was in inflation mode ~60% of time, and cycled off for a maximum time of about 11 sec.

During a hand assisted laparoscopic procedure, the insufflator was in inflation mode~75% of time, and cycled off for a maximum time of about 5 sec. During the standard laparoscopic procedure, with a slow continuous leak at the stop cock, with the insufflator set at a flow of 5-6 liters per minute and 12-13 mm HG, the insufflator remained in inflation mode 100% of time. During the standard laparoscopic procedure, with a slow continuous leak through a 16G angiocath, with the insufflator set at a flow of 5 liters per minute and 12-17 mm HG, the insufflator remained in inflation mode 100% of time.

During the standard surgical procedure, without hand assist, the scope was removed from the patient several times, for the reasons and durations as follows: Fog 40 sec; Fog 40 sec; Blood 40 sec; Fog 30 sec; Cautery 25 sec; Cautery 30 sec; Fog 30 sec; and Fog 25 sec. During the standard surgical procedure, with hand assist, the scope was removed from the patient several times, for the reasons and durations as follows: Fog 30 sec; Fog 60 sec; Cautery 25 sec; Cautery 25 sec; Debris 25 sec; Fog 60 sec; Fog 45 sec; Fog 30 sec; and Fog 30 sec.

Example 2

Evaluation of Fogging

In a device that simulates the humidity and temperature conditions of an animal abdominal cavity during a laparoscopic procedure, the effects of fogging on a laparoscopic lens was evaluated. Chamber temperature of 99.4-99.7° F., and an initial scope lens temperature of 70.1-72.1° F., humidity was 75-77% RH. FIG. 8 shows the change in scope temperature at the lens and various locations along its length at various times at the chambers humidity.

Relative humidity is understood as the Ratio of water vapor (dew point). Above the line corresponding to the relative humidity in the chamber, no condensation is observed; below the line, condensation is observed. The principle was observed in the study, wherein, upon initial insertion of the scope into the chamber, fogging immediately occurred and visualization of an object in the chamber was obscured. It was

observed that visualization of the object improved as the scope heated up above dew point temperature, and condensation dissipated.

Example 3

Evaluation of Accumulator Reservoir Function

Testing was performed in a simulator as described in EXAMPLE 2 to compare insufflator function with and with out an accumulator. The conditions of testing were similar for each trial, with chamber temperature of 99.4-99.7° F., and an initial scope lens temperature of 70.1-72.1° F., humidity was 75-77% RH.

The defogging threshold was determined in later testing. A valve was placed inline with an embodiment of the view optimizer described herein and attached to a compliant reservoir. This valve was slowly closed until the airflow was restricted to the point where defogging did not occur. Two trials were performed with the chamber temperature being 102.9-103.9° F. with an initial scope lens temperature of 70.5-70.9° F., humidity was 75-76% RH. Observation of the data recorder showed that at steady state, the maximum peak flow was registered at 1.3V during this time. The voltage of the sensor at 0 flow was measured pretest at 1.228V. FIG. 9 shows the resulting data, wherein the use of an accumulator reservoir compensated for the insufflator to deliver a continuous stream of air when the insufflator was shut-off, and a shift in flow was observed upon re-initiation of insufflator function until the complaint reservoir was replenished with gas.

The embodiments and examples of the view optimizer 200 described herein are representative of aspects of the invention and are provided as examples and not an exhaustive description of implementations of an aspect of the invention. While various aspects of the view optimizer 200 are described and illustrated herein as embodied in combination in the exemplary embodiments, these various aspects may be realized in many alternative embodiments, either individually or in various combinations and sub-combinations thereof. Unless expressly excluded herein all such combinations and sub-combinations are intended to be within the scope of the present application. Still further, while various alternative embodiments as to the various aspects and features of the invention, such as alternative materials, structures, configurations, methods, devices, such descriptions are not intended to be a complete or exhaustive list of available alternative embodiments, whether presently known or later developed. Those skilled in the art may readily adopt one or more of the aspects, concepts or features of the invention into additional embodiments within the scope of the present invention even if such embodiments are not expressly disclosed herein. Additionally, even though some features, concepts or aspects of the invention may be described herein as being a preferred arrangement or method, such description is not intended to suggest that such feature is required or necessary unless expressly so stated.

The invention claimed is:

1. A view optimizing assembly for use with a laparoscope having an objective lens for viewing a body cavity insufflated with CO₂ by an insufflator, the assembly comprising a cylindrical tube separate from the laparoscope and having a distal end, the cylindrical tube having an interior lumen

configured to accommodate passage of the laparoscope to position the objective lens generally adjacent to the distal end during use and to accommodate removal of the laparoscope from the cylindrical tube after use, the cylindrical tube including a pair of first interior channels, and a second interior channel separate from the pair of first interior channels, a lens guard projecting circumferentially forward and beyond the distal end of the cylindrical tube and including a pair of first passages formed in the lens guard communicating with the pair of first interior channels and not the second interior channel, and a second passage formed in the lens guard communicating with the second interior channel and not the pair of first interior channels, a first supply conduit having tubing configured to couple with the insufflator to divert a portion of the CO₂ from the insufflator into the pair of first interior channels and through the pair of first passages so as to direct a stream of diverted CO₂ across the objective lens at a diverted flow rate of at least 0.07 liters per minute in a plurality paths to defog the objective lens and deflect debris, a second supply conduit configured to couple with a source of liquid, the second supply conduit coupled with a manually controlled actuator configured to convey the liquid through the second supply conduit, into the second interior channel, and through the second passage so as to direct a stream of the liquid across the objective lens in a second path different than the plurality of first paths to clear material from the objective lens, wherein residual droplets of the liquid may remain on the objective lens that are resistant to removal by the stream of diverted CO₂ directed across the objective lens at the diverted flow rate, and a manually activated pneumatic bulb coupled with the first supply conduit and configured to deliver a burst of CO₂ through the pair of first interior channels, through the pair of first passages, and across the objective lens at a burst flow rate greater than the diverted flow rate to remove the residual droplets of the liquid from the objective lens.

2. An assembly according to claim 1 wherein the lens guard is angled to correspond with a laparoscope having an angled end portion.

3. An assembly according to claim 1 wherein the cylindrical tube comprises a rigid material.

4. An assembly according to claim 1 wherein the cylindrical tube comprises a flexible material.

5. An assembly according to claim 1 wherein the diverted flow rate is upwards to 10 liters per minute.

6. An assembly according to claim 1 wherein the lens guard projects forward and beyond the distal end of the cylindrical tube by upwards to 7 mm.

7. An assembly according to claim 5 wherein the burst flow rate is greater than or equal to 20 liters per minute.

* * * * *

专利名称(译) 用于保持手术范围可视化的装置

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摘要(译)

本申请公开了用于维持外科手术范围的可视化的装置的若干实施例。当外科手术室用于在患者体内进行外科手术时，该装置的实施例适于屏蔽，除雾或清洁手术镜的镜片。在一个实施例中，提供了一种视图优化器，其适于将至少一种流体输送到腹腔镜的物镜，以清洁和/或除去腹腔镜的物镜，而无需从手术区域移除腹腔镜。在另外的实施例中，提供了一种视图优化器，其适于产生来自体腔的气体泄漏或排出，以确保来自吹入器的连续气体流动。

