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Engeberg et al.(10) **Pub. No.: US 2014/0074084 A1**(43) **Pub. Date: Mar. 13, 2014**(54) **VARIABLE-FREQUENCY STIMULATOR FOR ELECTROSURGERY**(75) Inventors: **Erik Engeberg**, Cuyahoga Falls, OH (US); **Eric Espinal**, Akron, OH (US)(73) Assignee: **THE UNIVERSITY OF AKRON**, Akron, OH (US)(21) Appl. No.: **14/115,481**(22) PCT Filed: **May 4, 2012**(86) PCT No.: **PCT/US12/36532**

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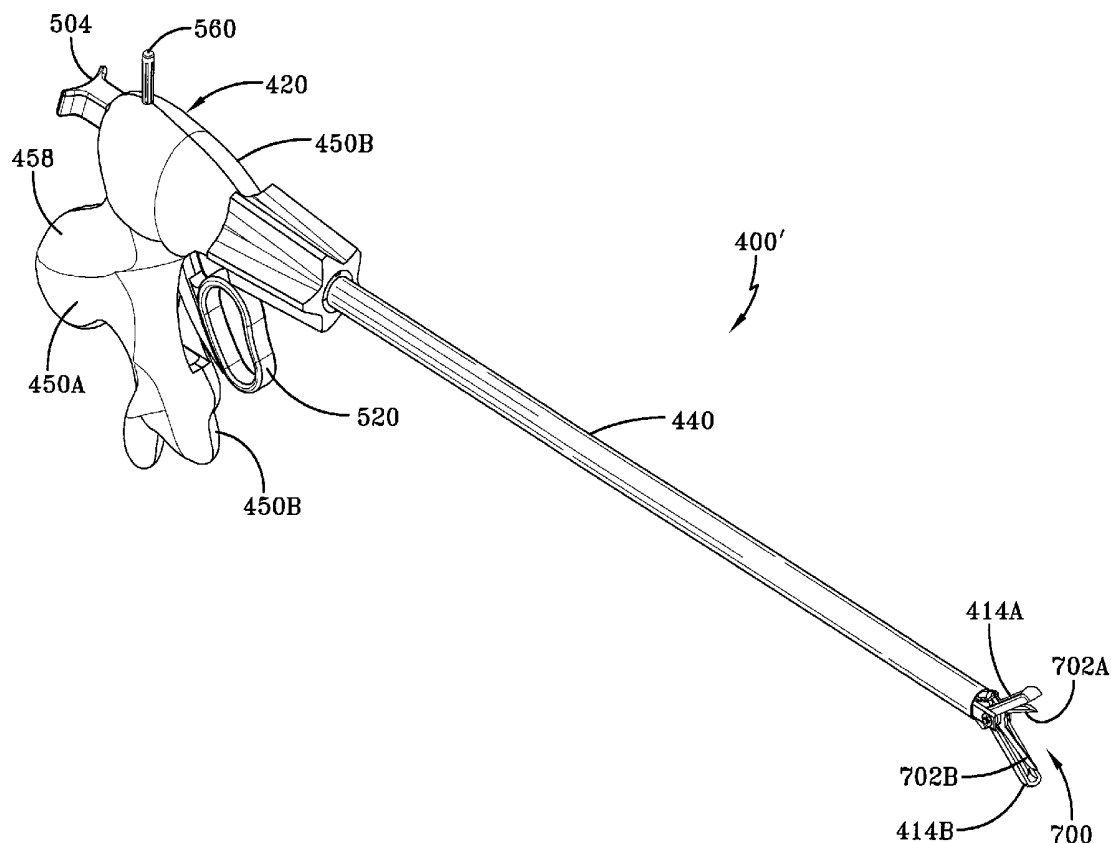
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(57)

ABSTRACT

A variable-frequency stimulator for electrosurgery includes an impedance analyzer to identify the electrical impedance of biological tissue being treated by an electrosurgical instrument, such as a laparoscope. Based on the identified tissue impedance, a controller adjusts the frequency of electrical current delivered to the electrosurgical instrument to reduce, minimize or normalize the impedance of the tissue, thereby preventing collateral damage to the tissue in and about the surgical site. Additionally, the laparoscope may be configured with multiple electrically conductive grasping arms that are used to deliver the electrical current to the surgical site. The conductive grasping arms provide multiple current paths for the electrical current to flow, thus concentrating the electrical current at the surgical site during an electrosurgical procedure. Thus, the unwanted spread of electrical current in the tissue is prevented, resulting in the reduction or prevention of collateral damage to tissue in and about the surgical site.



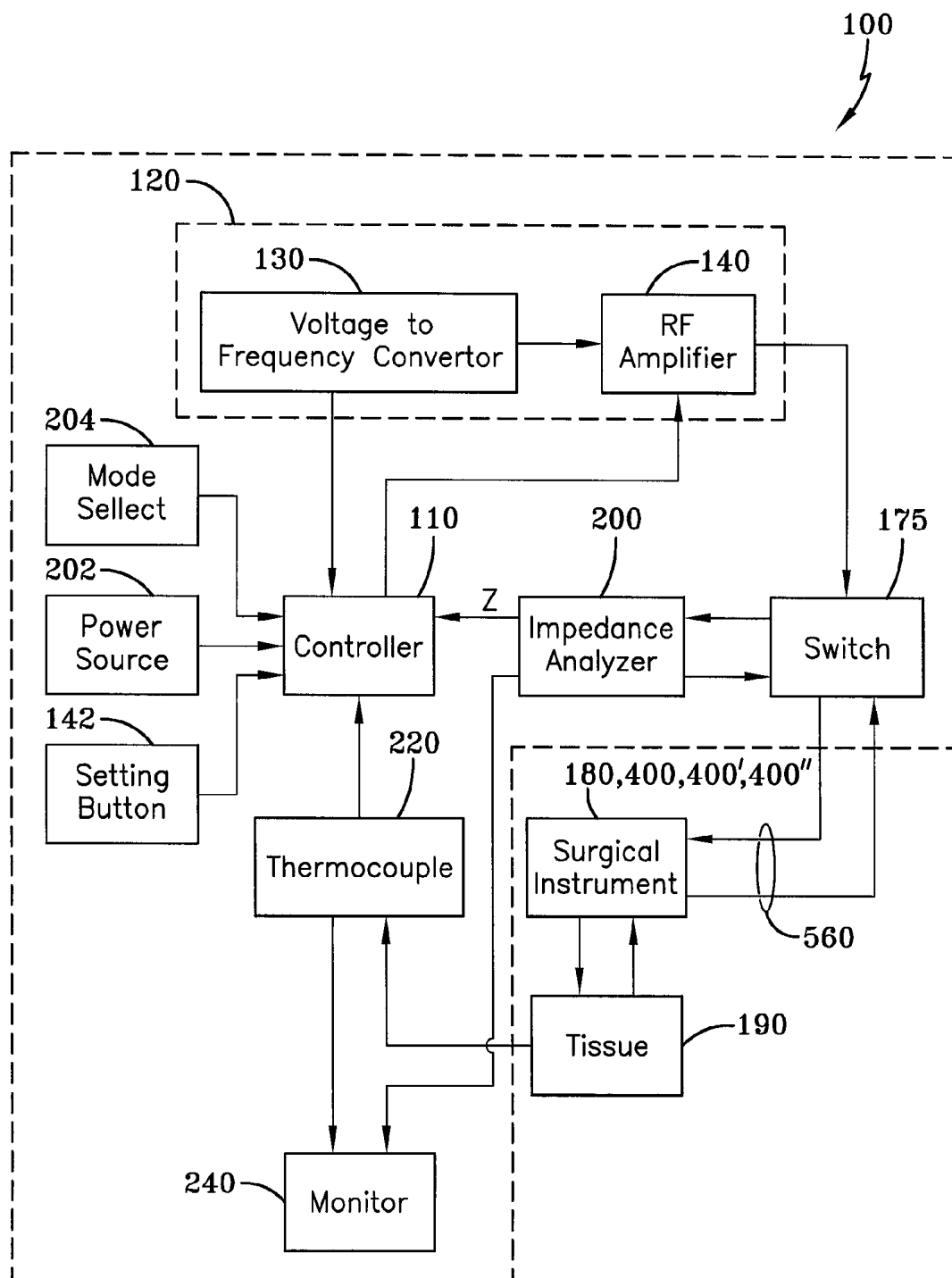
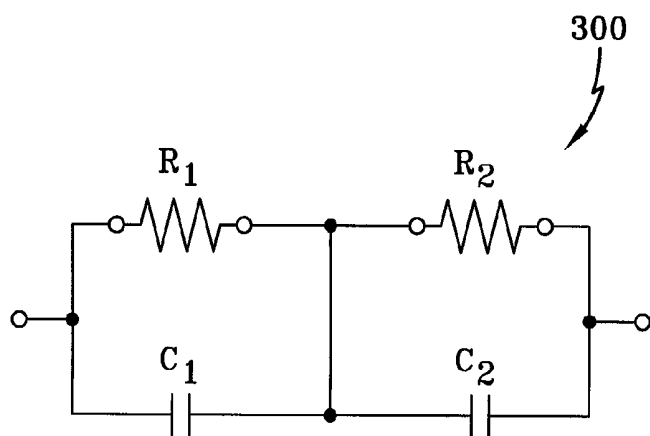
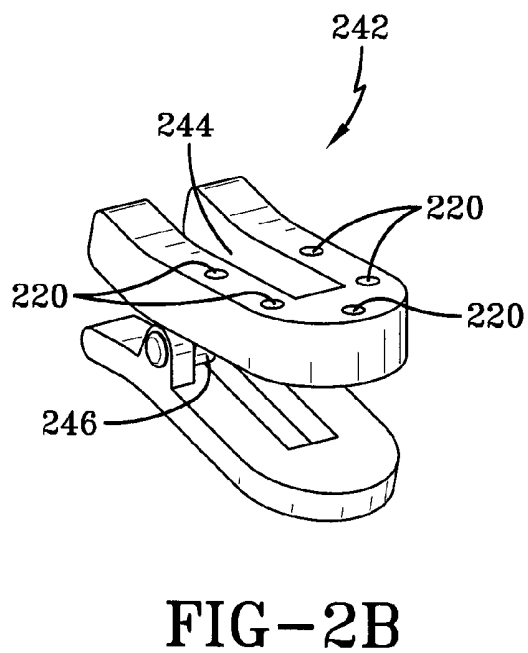
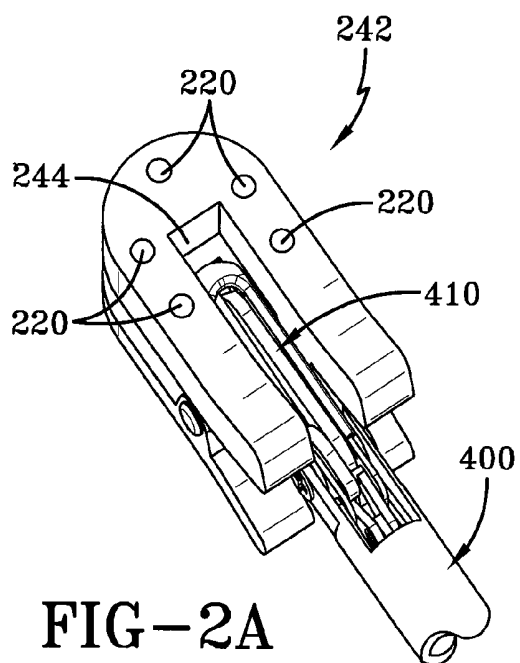


FIG-1



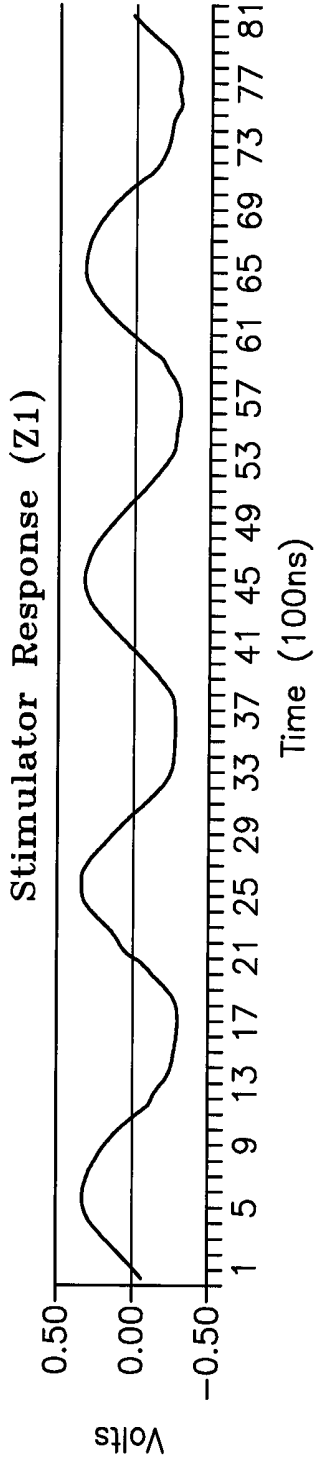


FIG-4

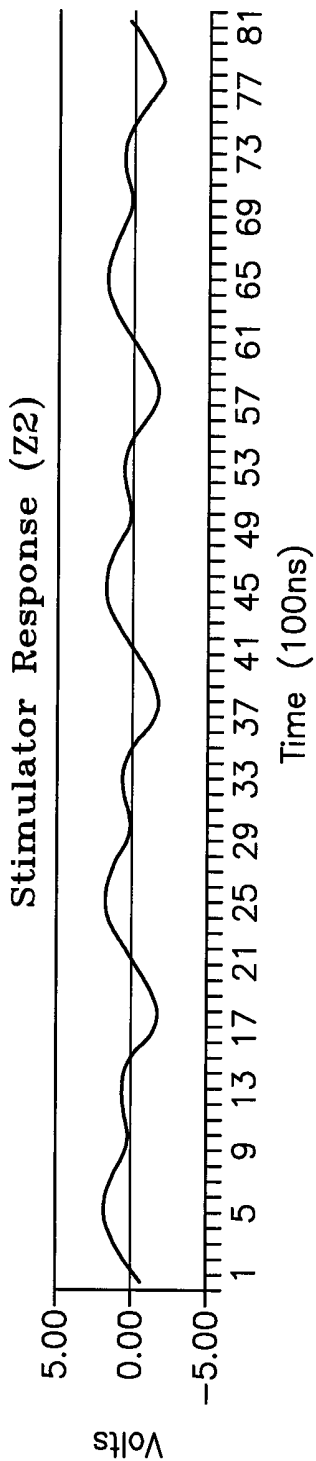


FIG-5

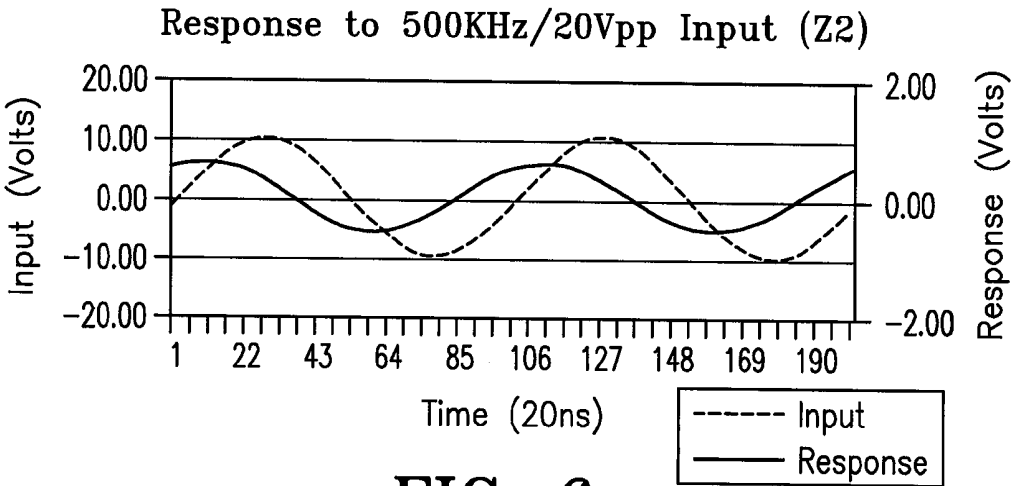


FIG-6

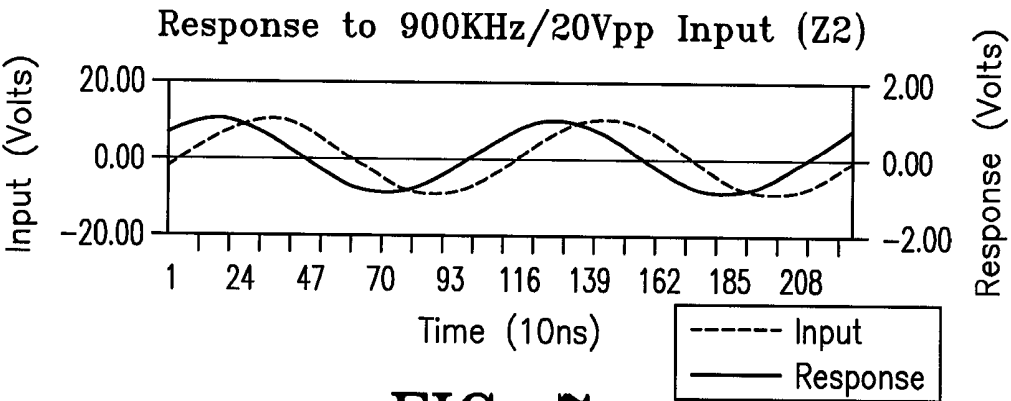


FIG-7

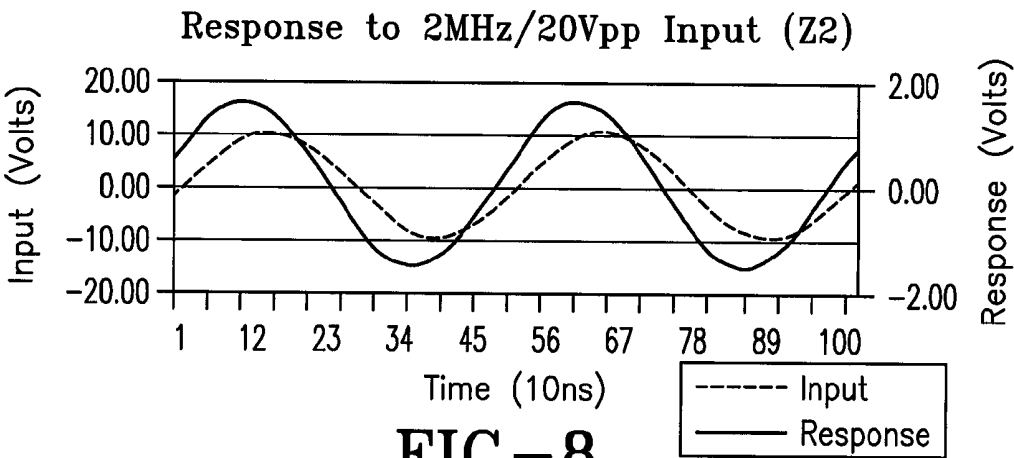
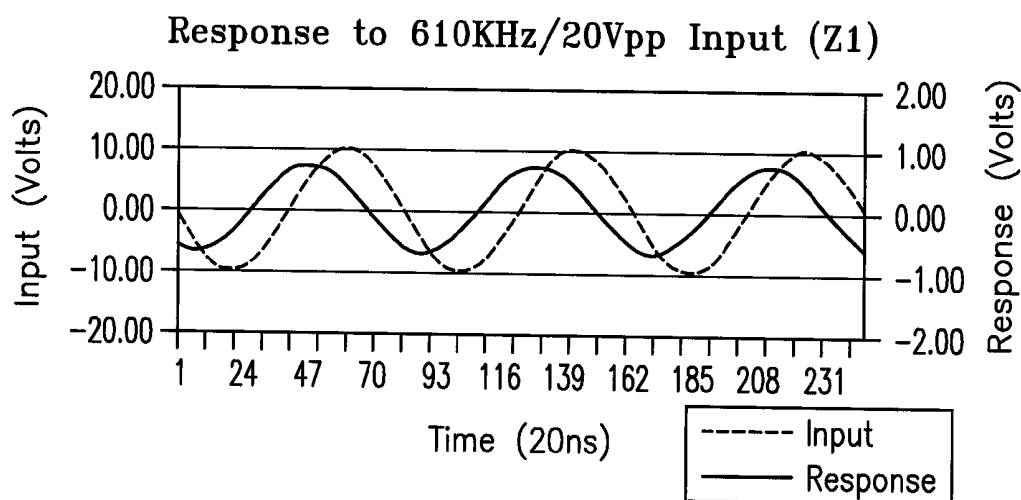
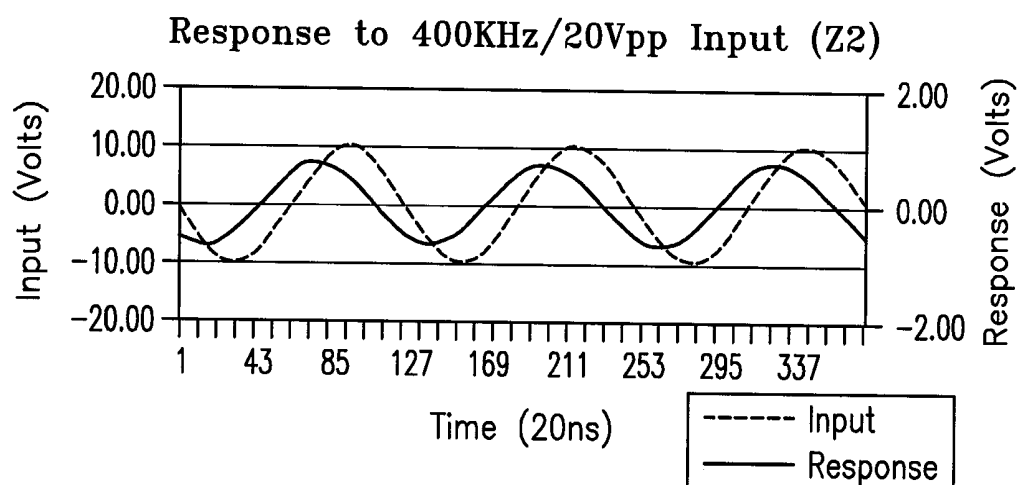
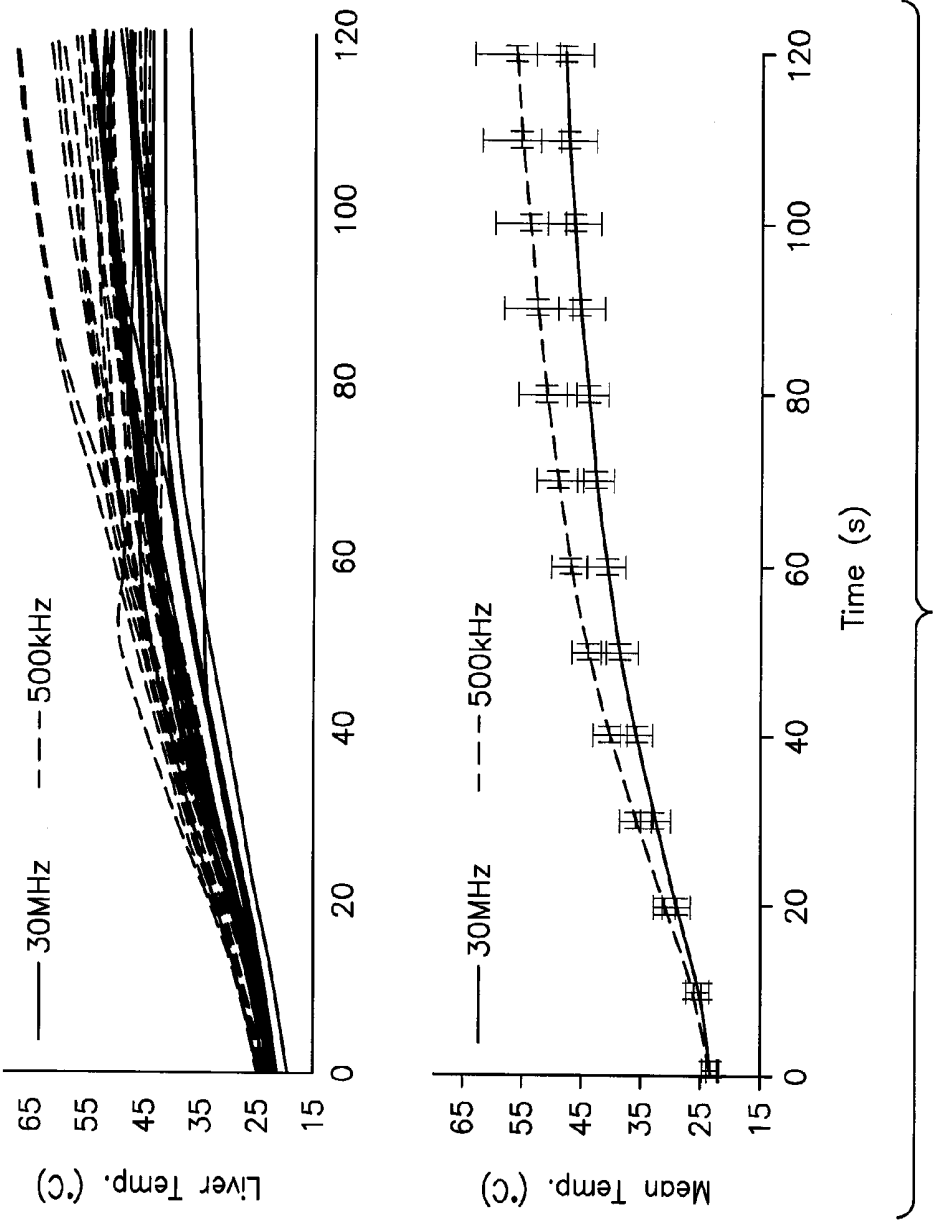


FIG-8

**FIG-9****FIG-10**



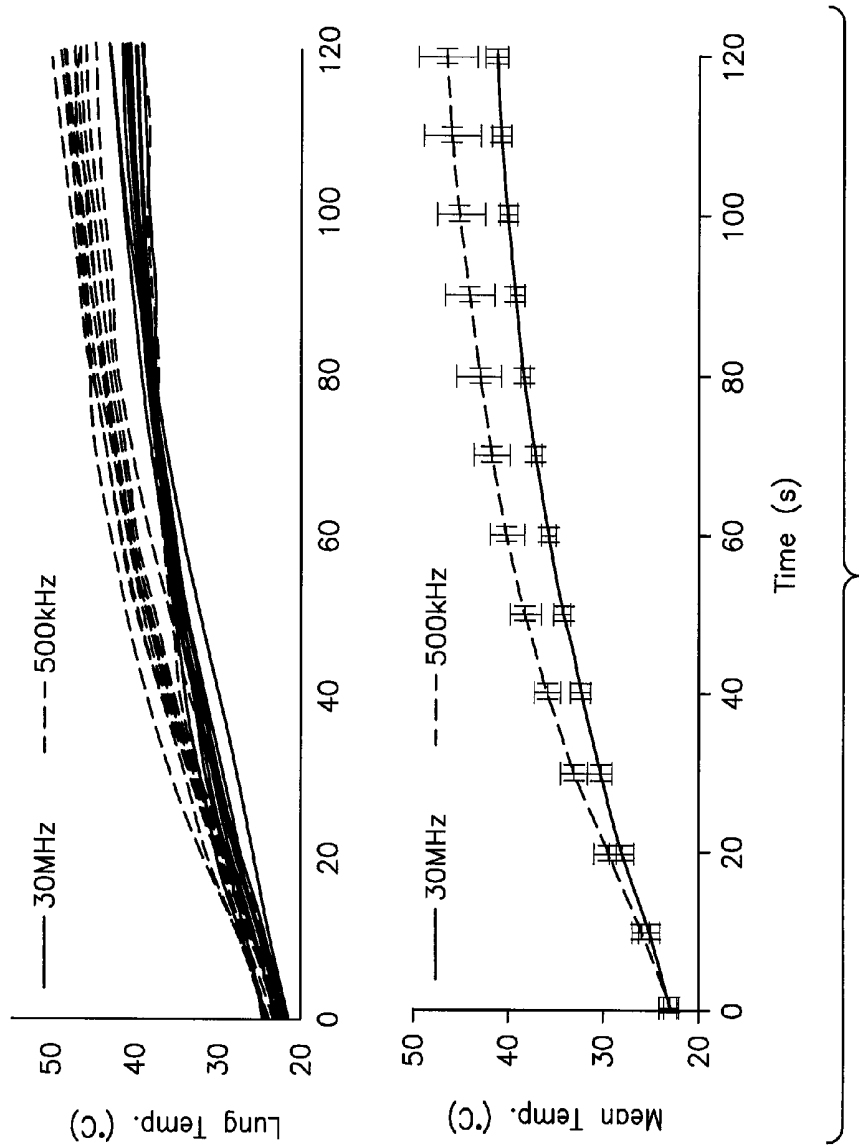


FIG-11B

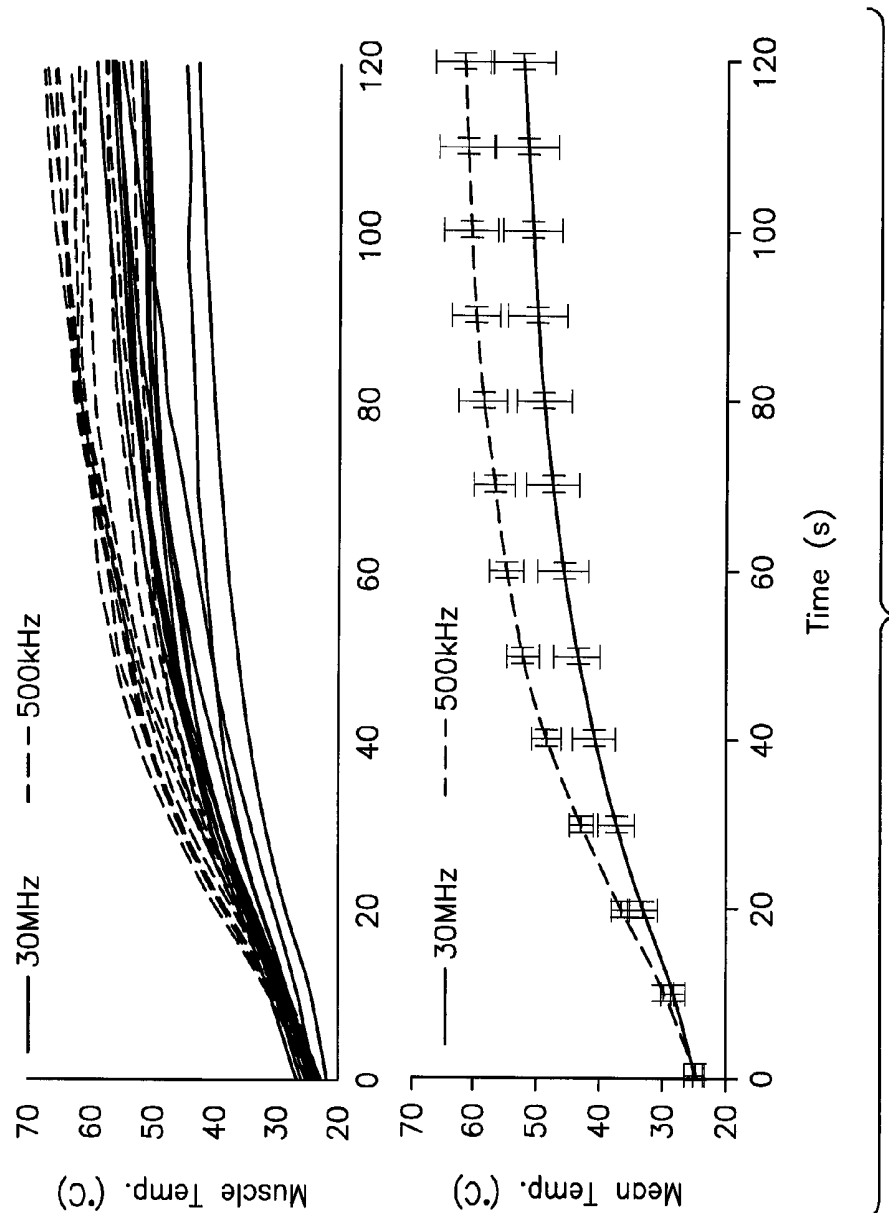
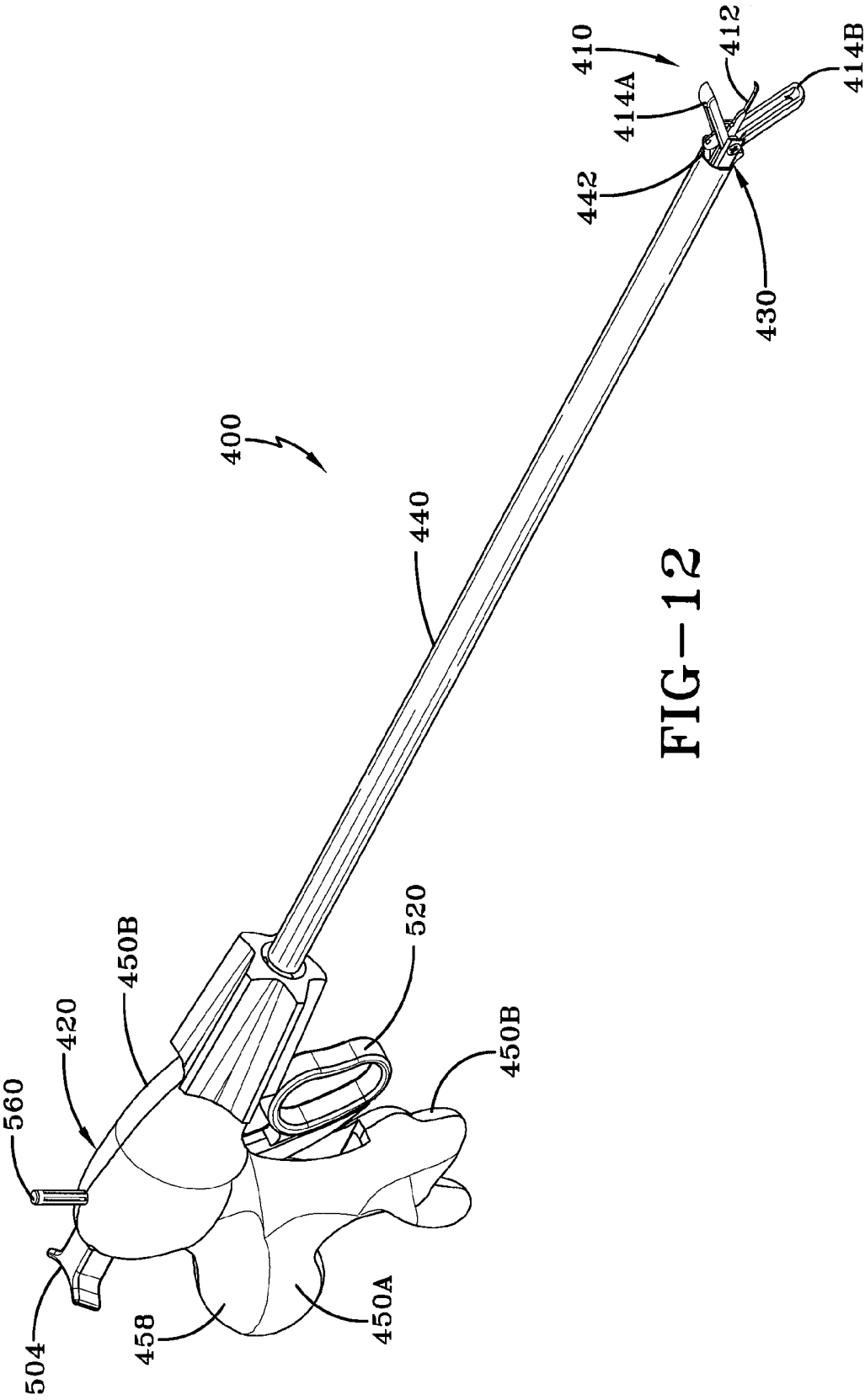
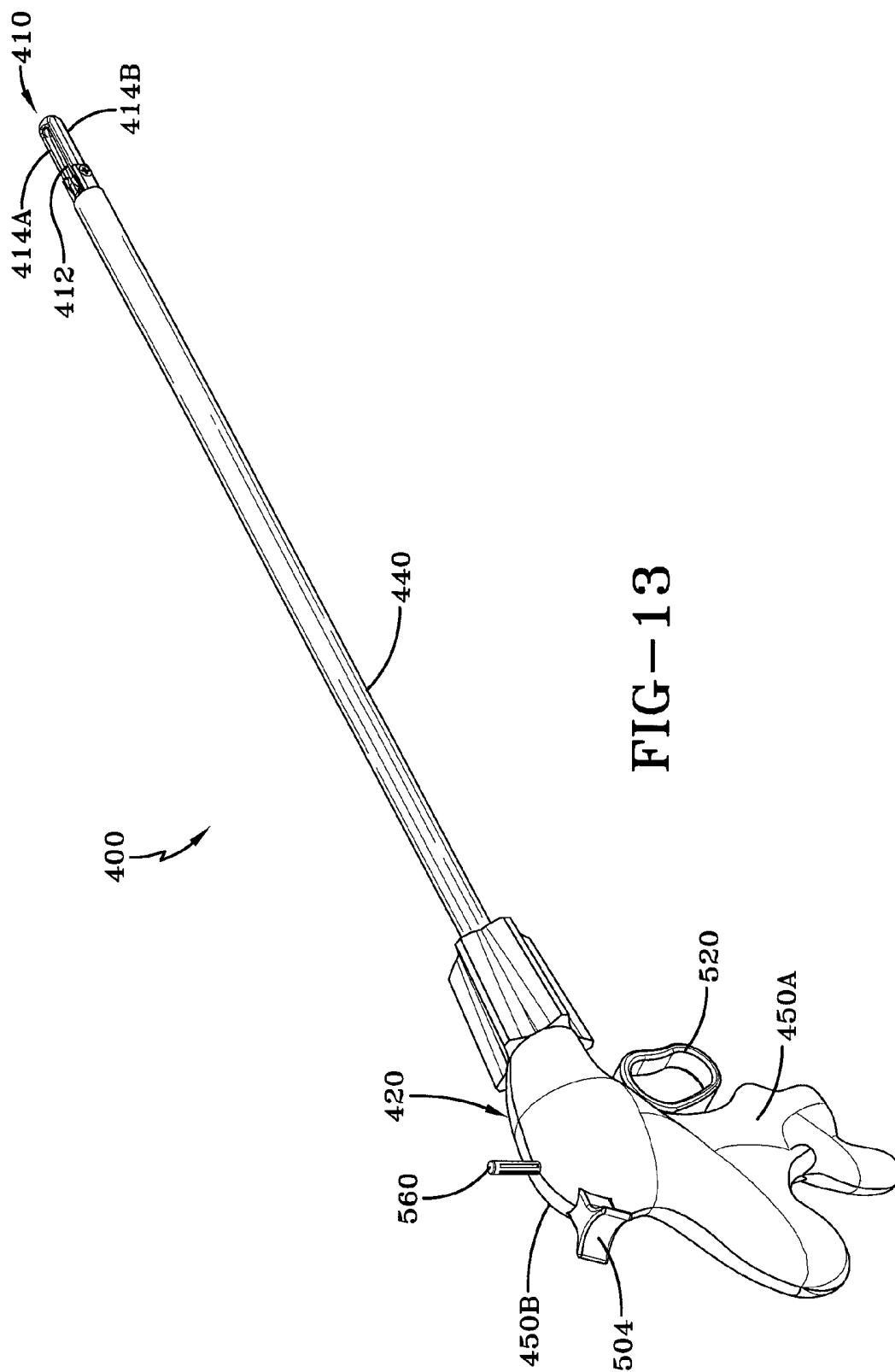


FIG-11C





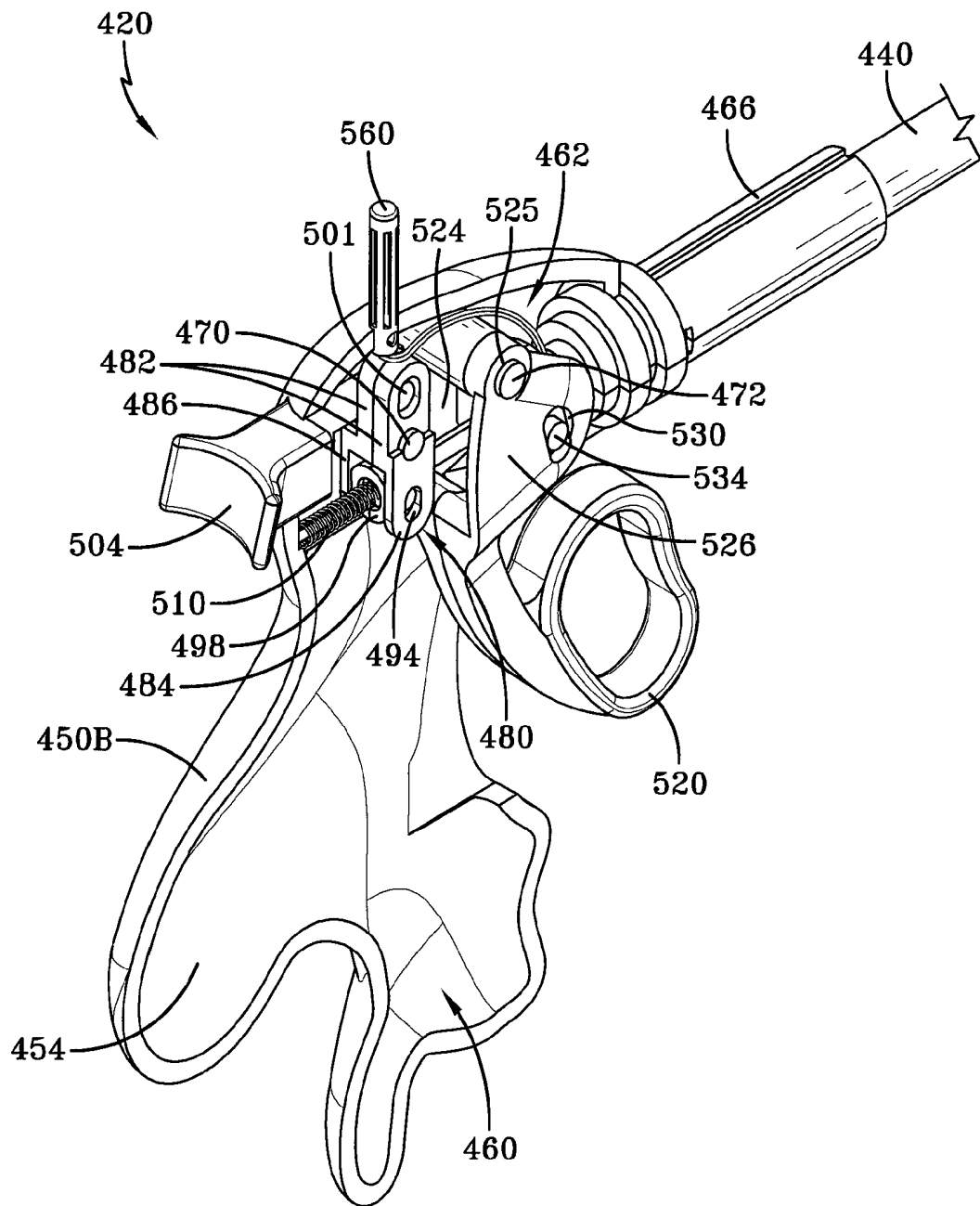


FIG-14A

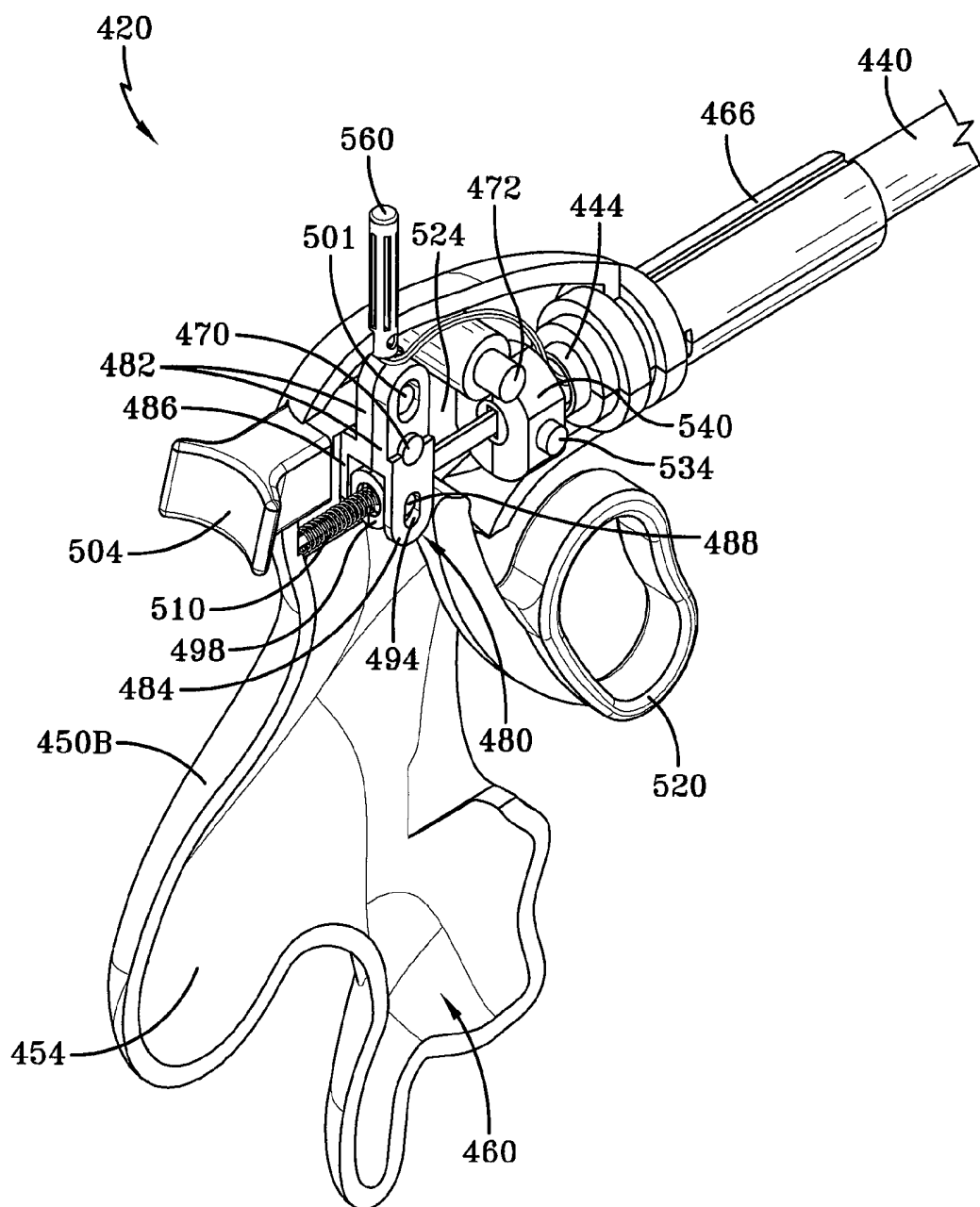


FIG-14B

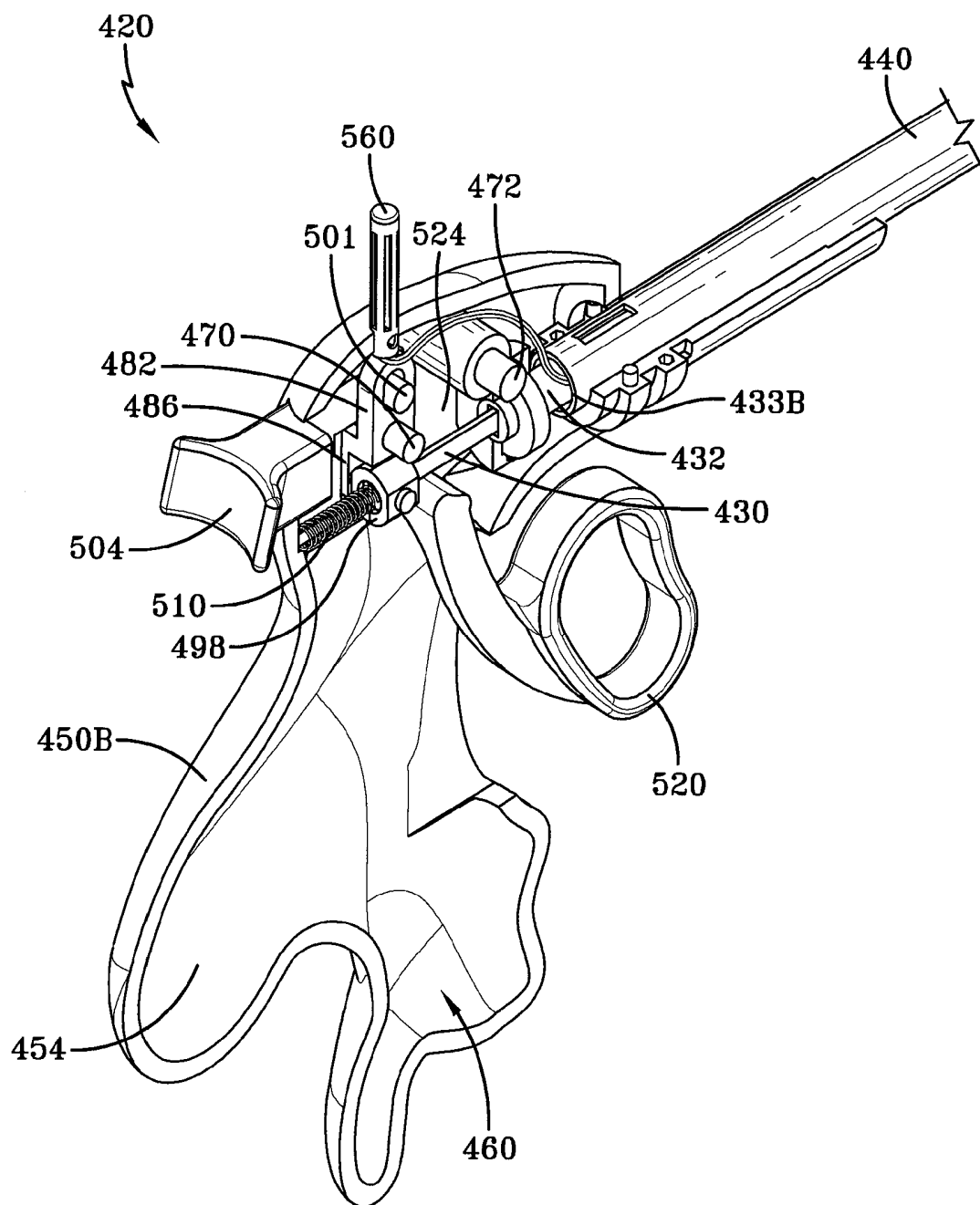


FIG-14C

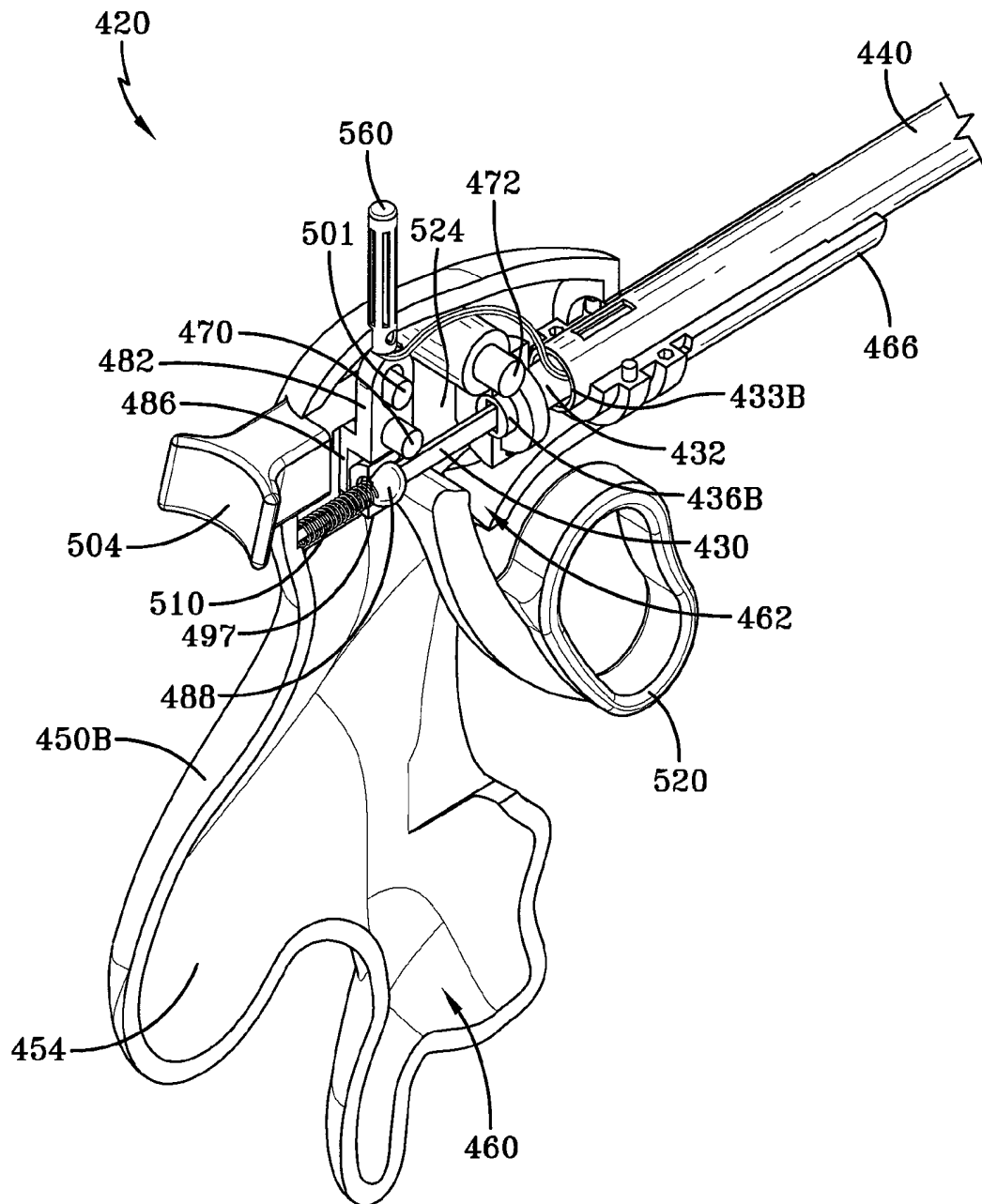


FIG-14D

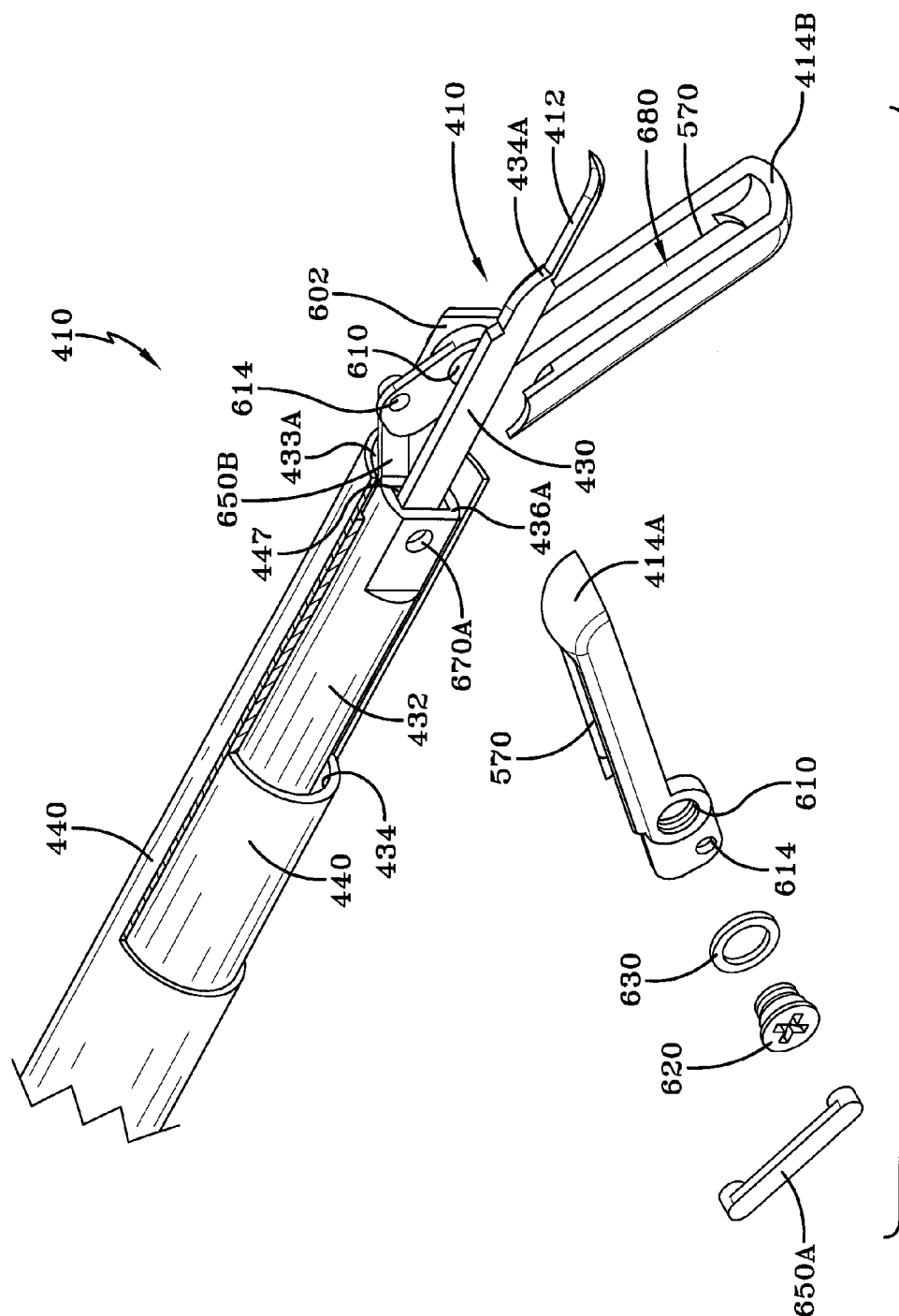
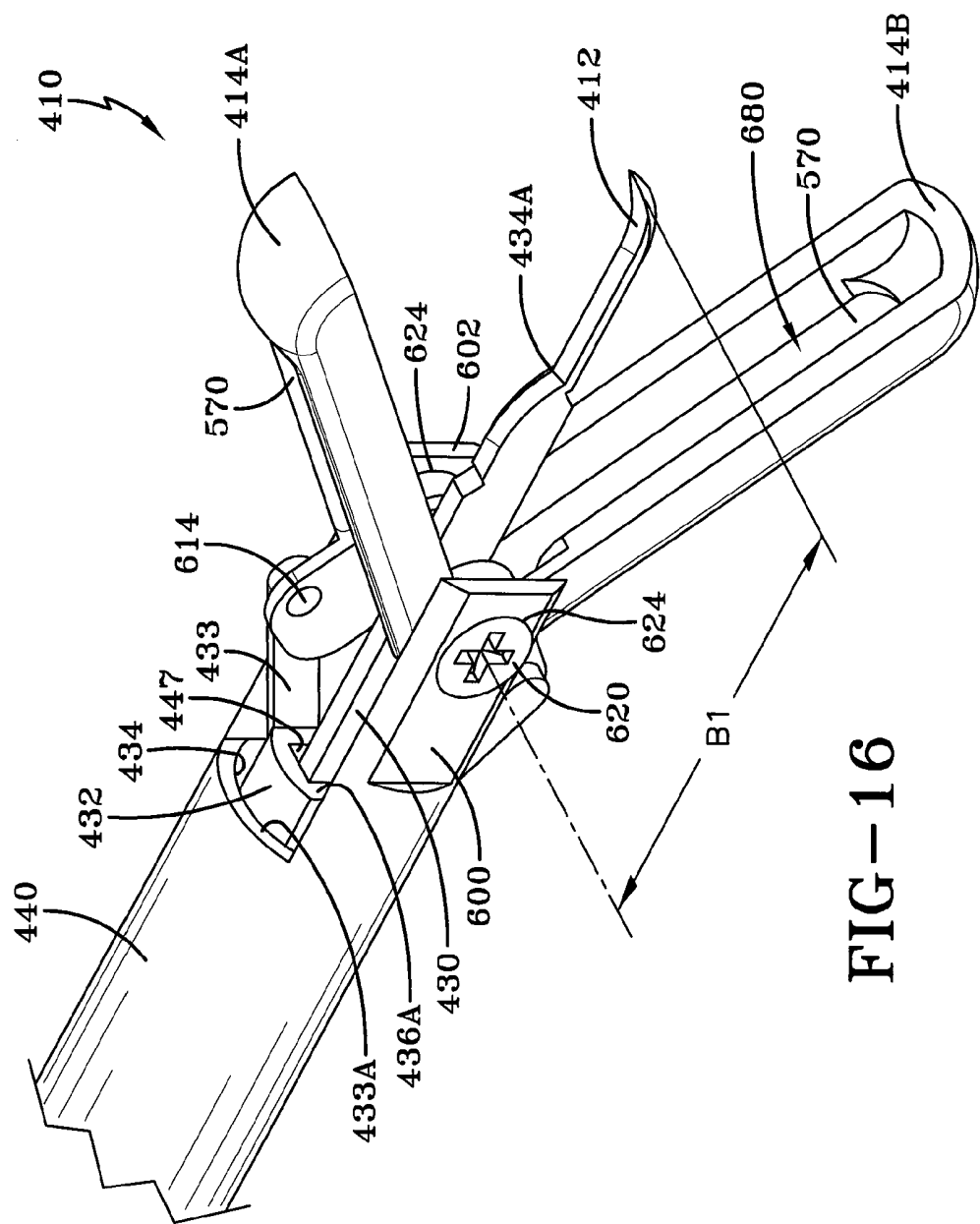


FIG-15



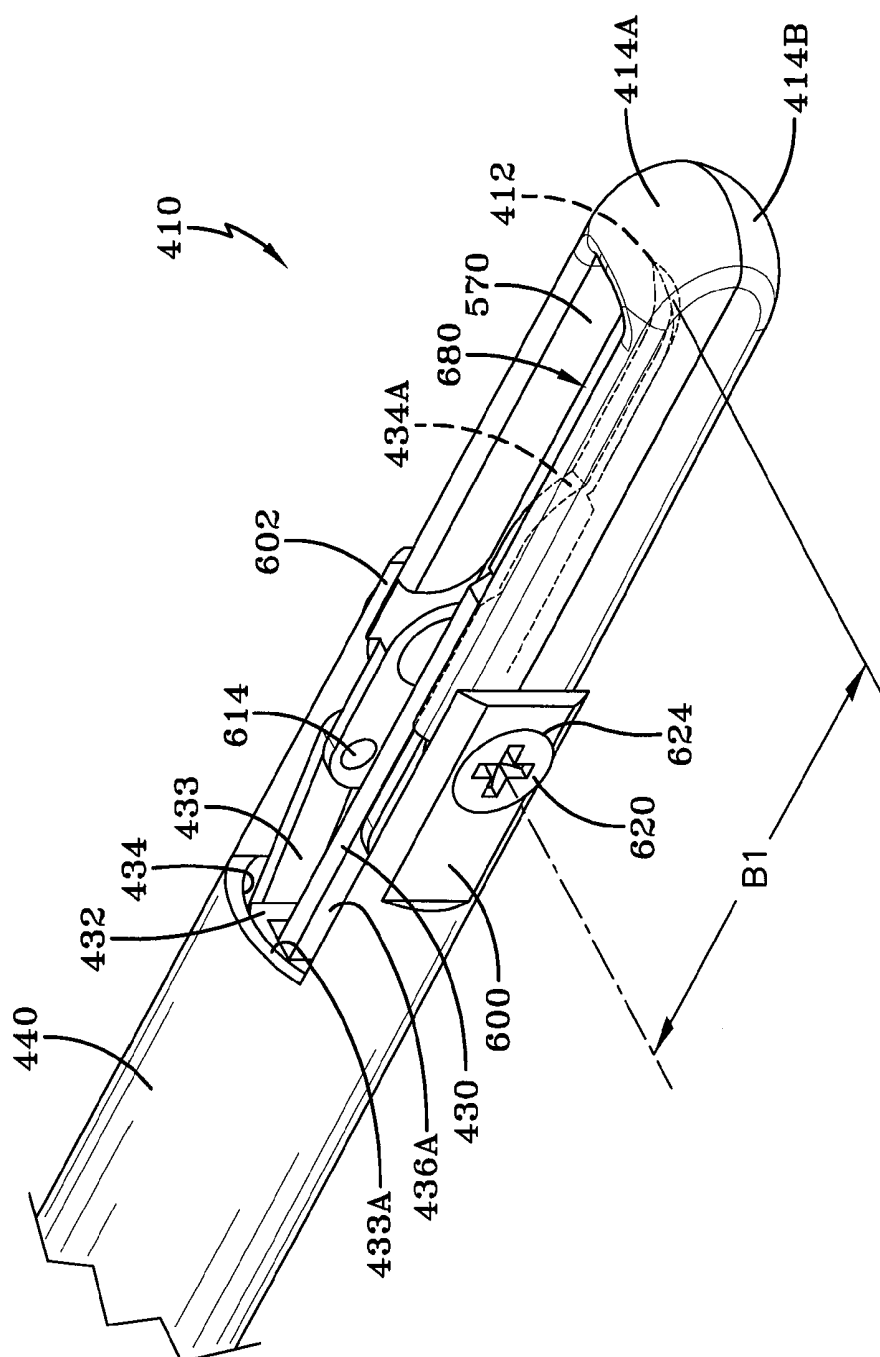


FIG-17

FIG-18A

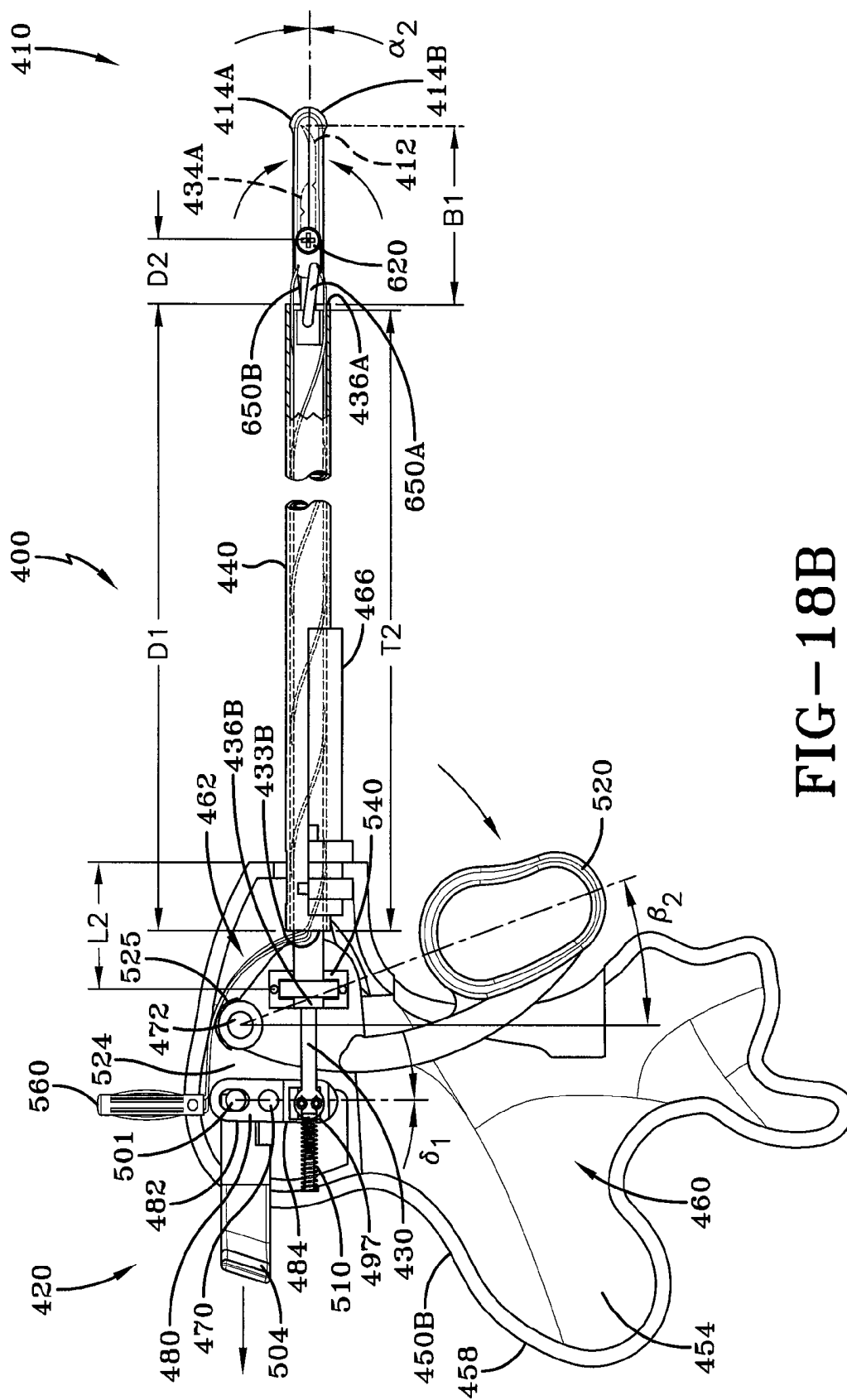


FIG-18B

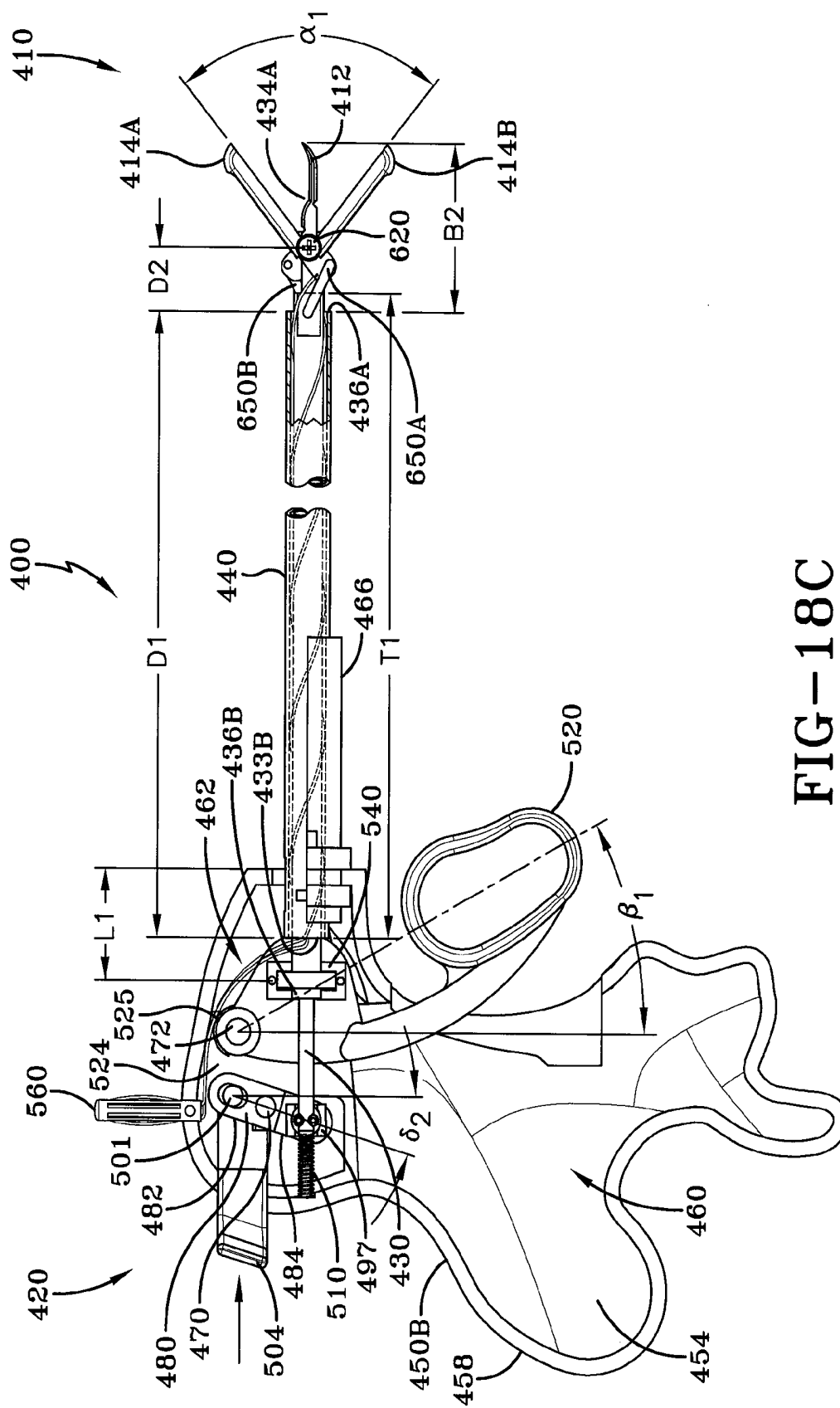
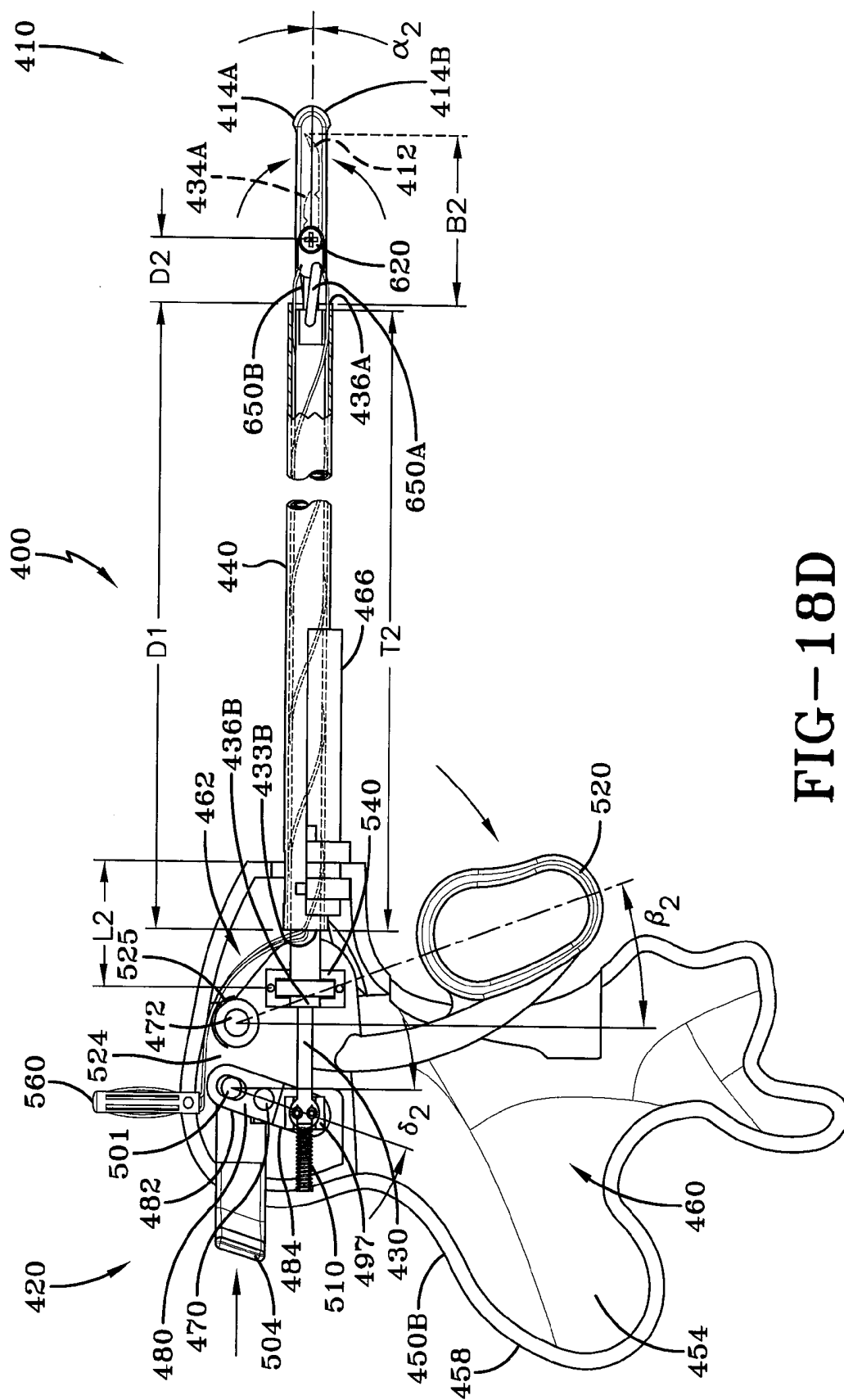
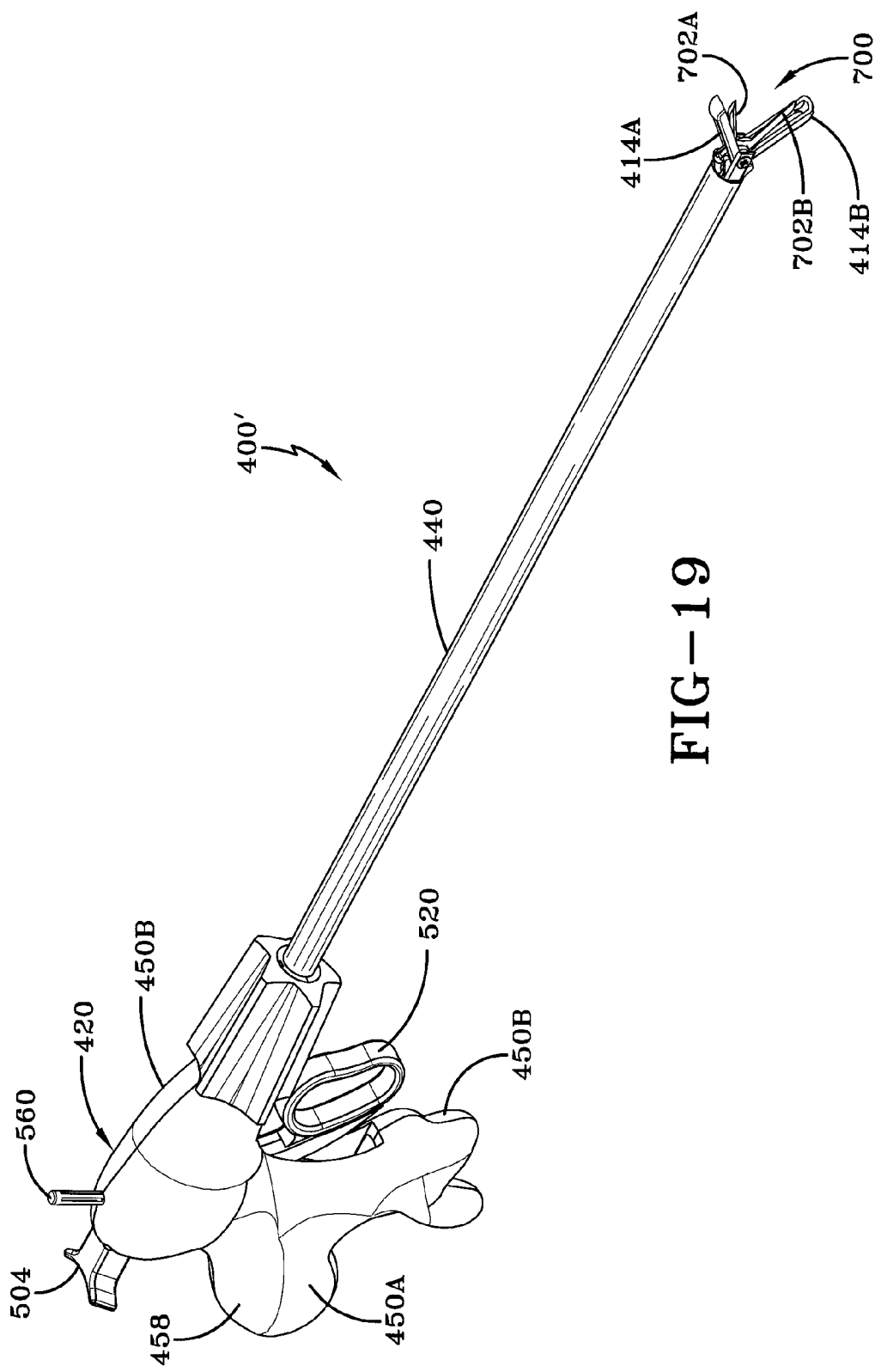
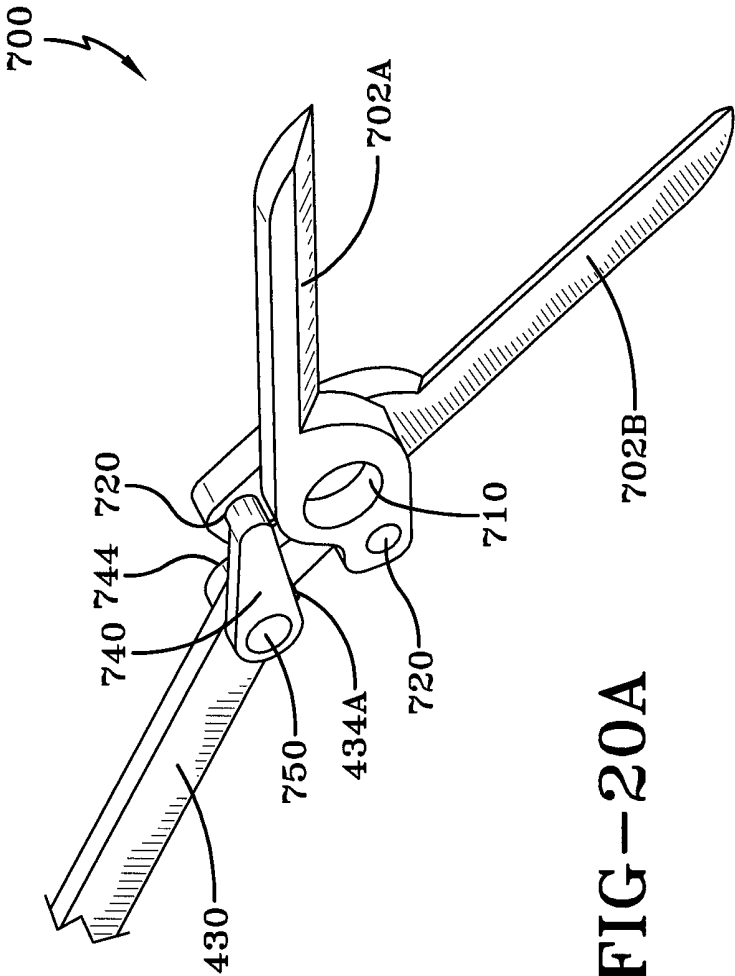
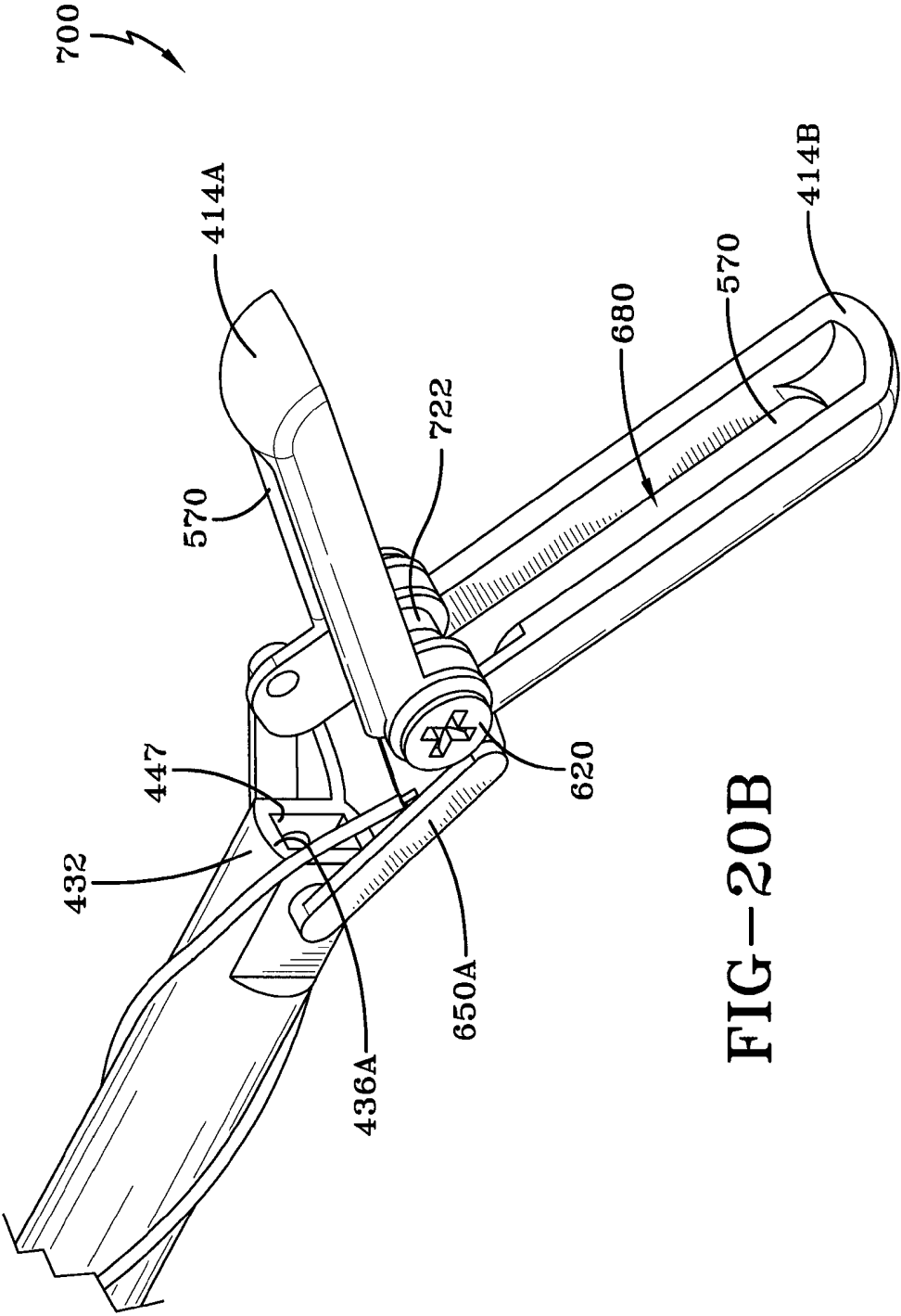


FIG-18C









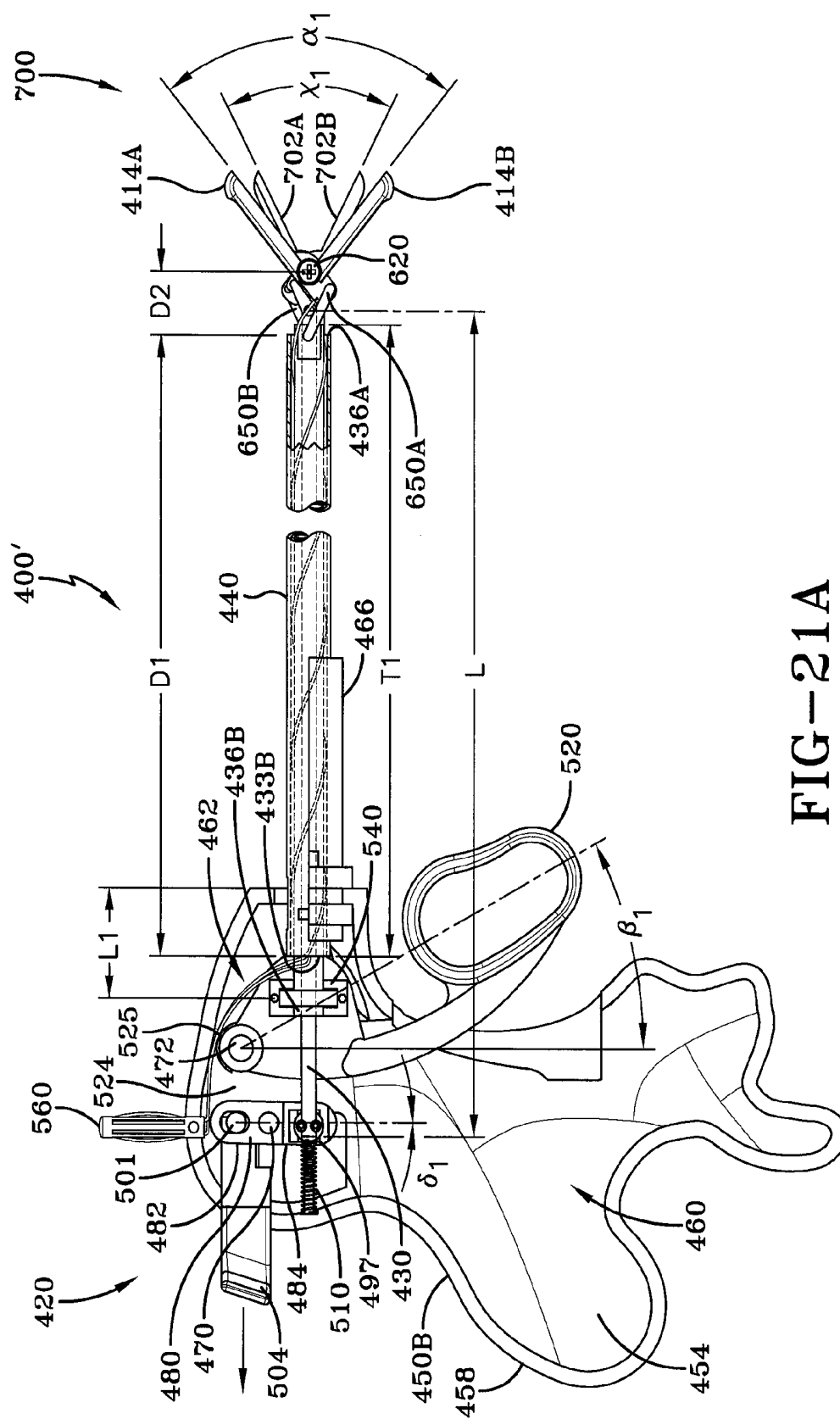
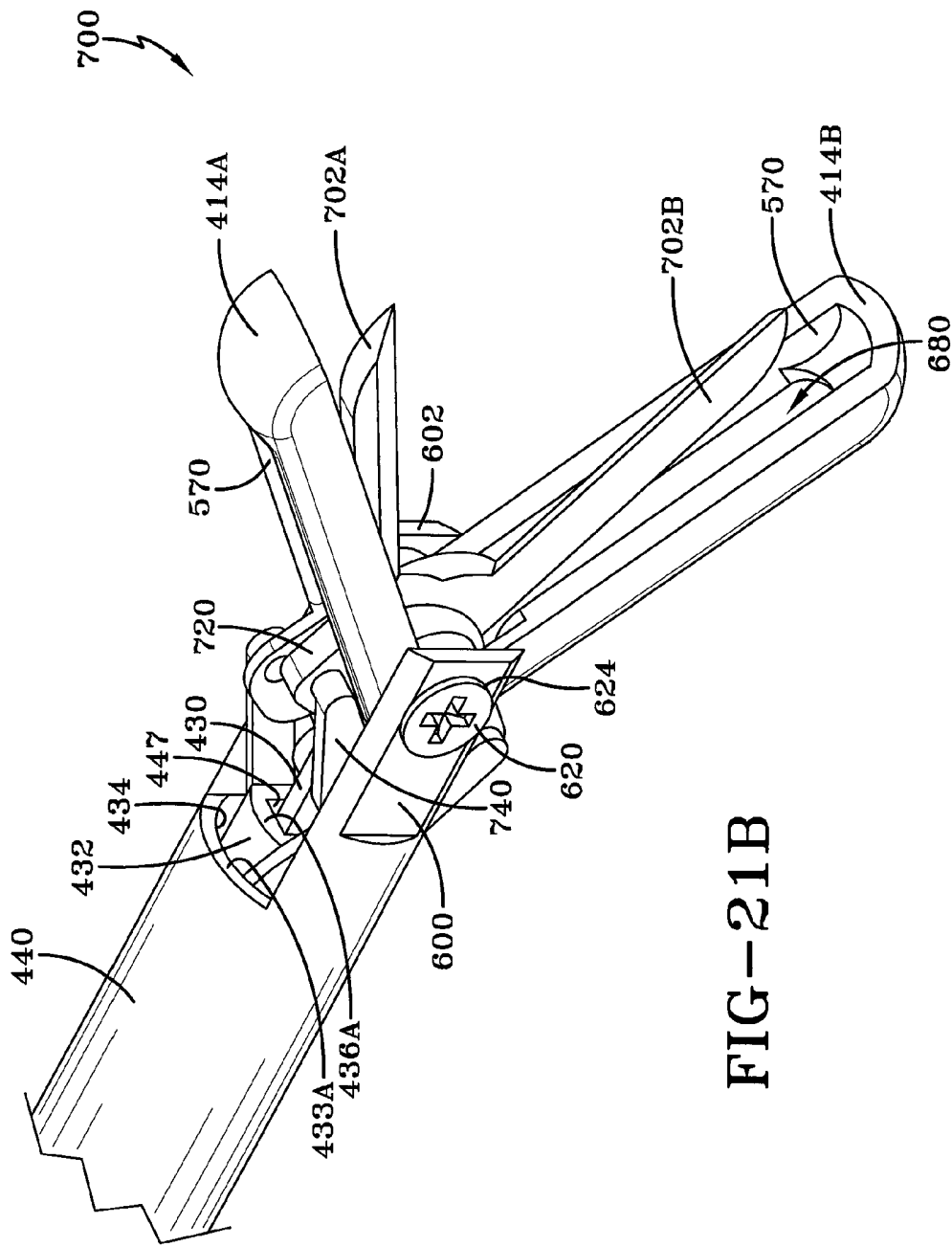


FIG-21A



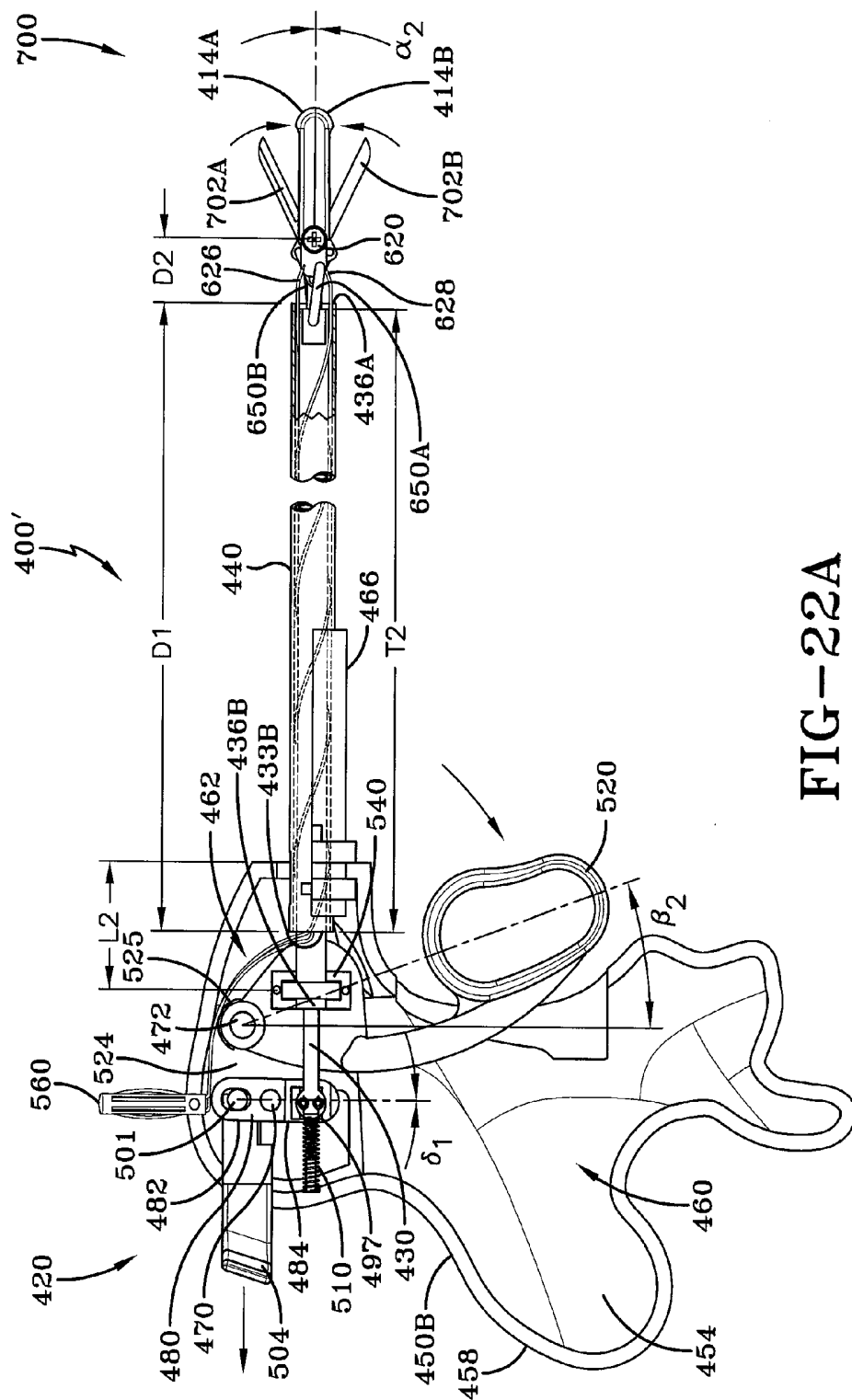
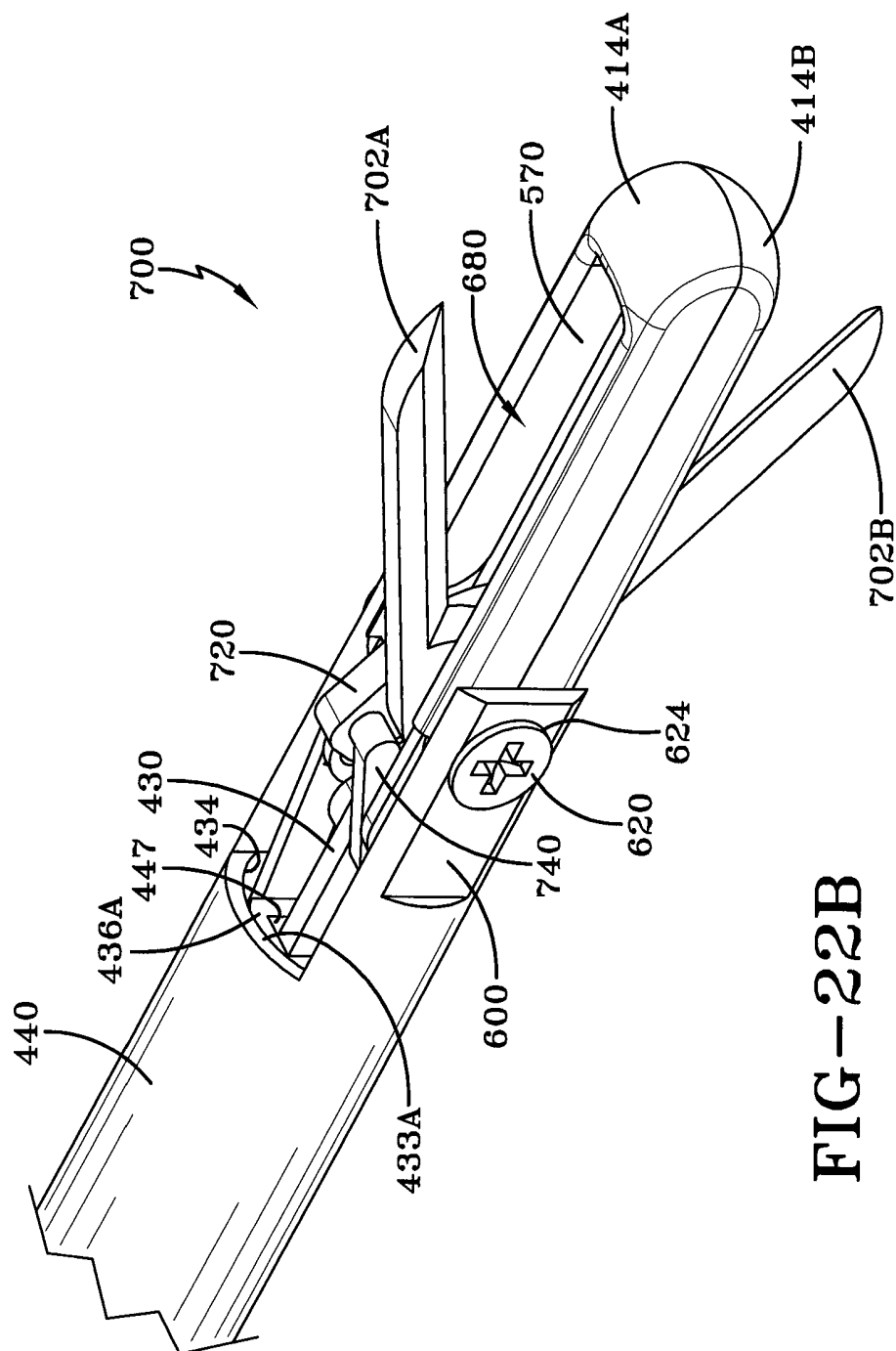


FIG-22A



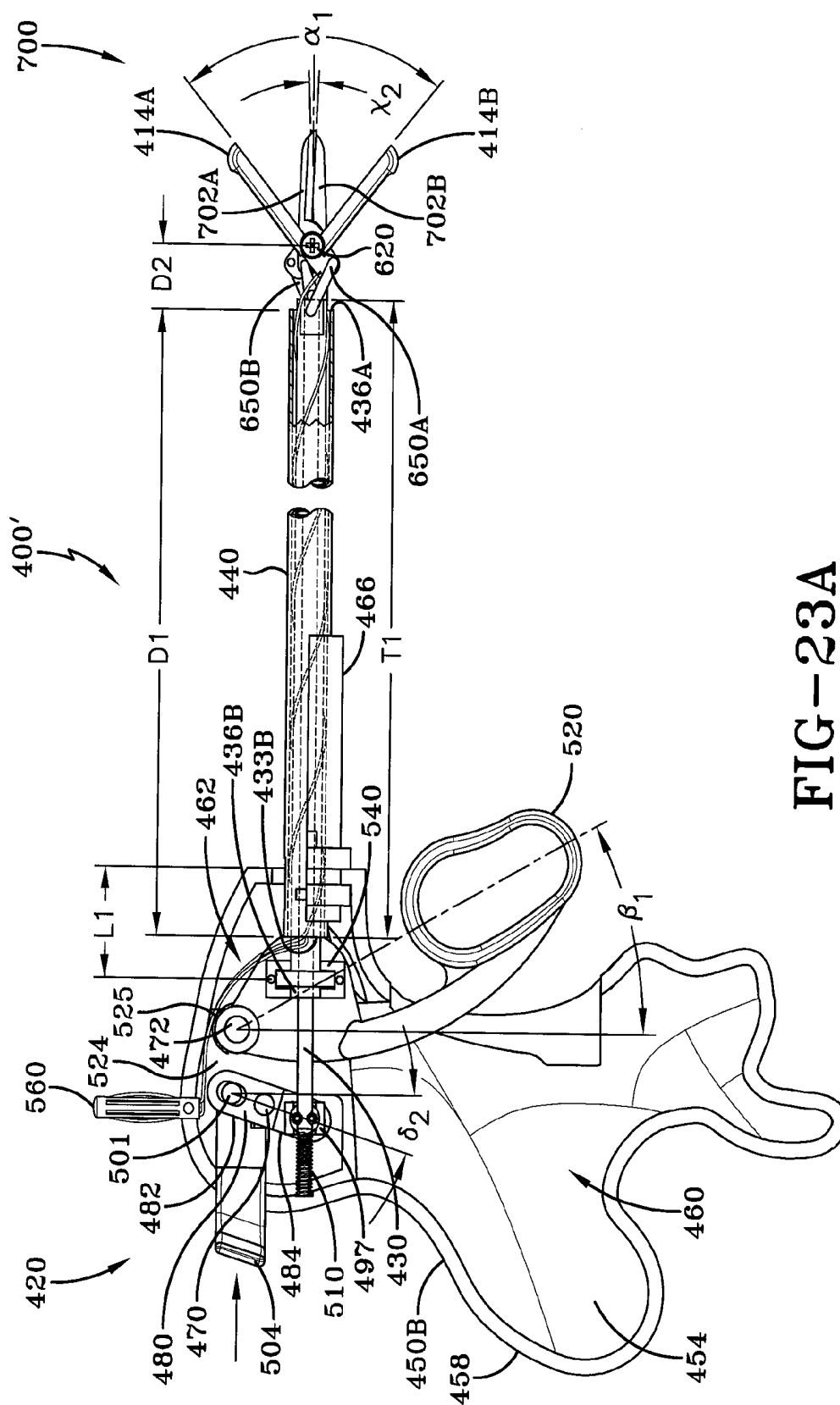
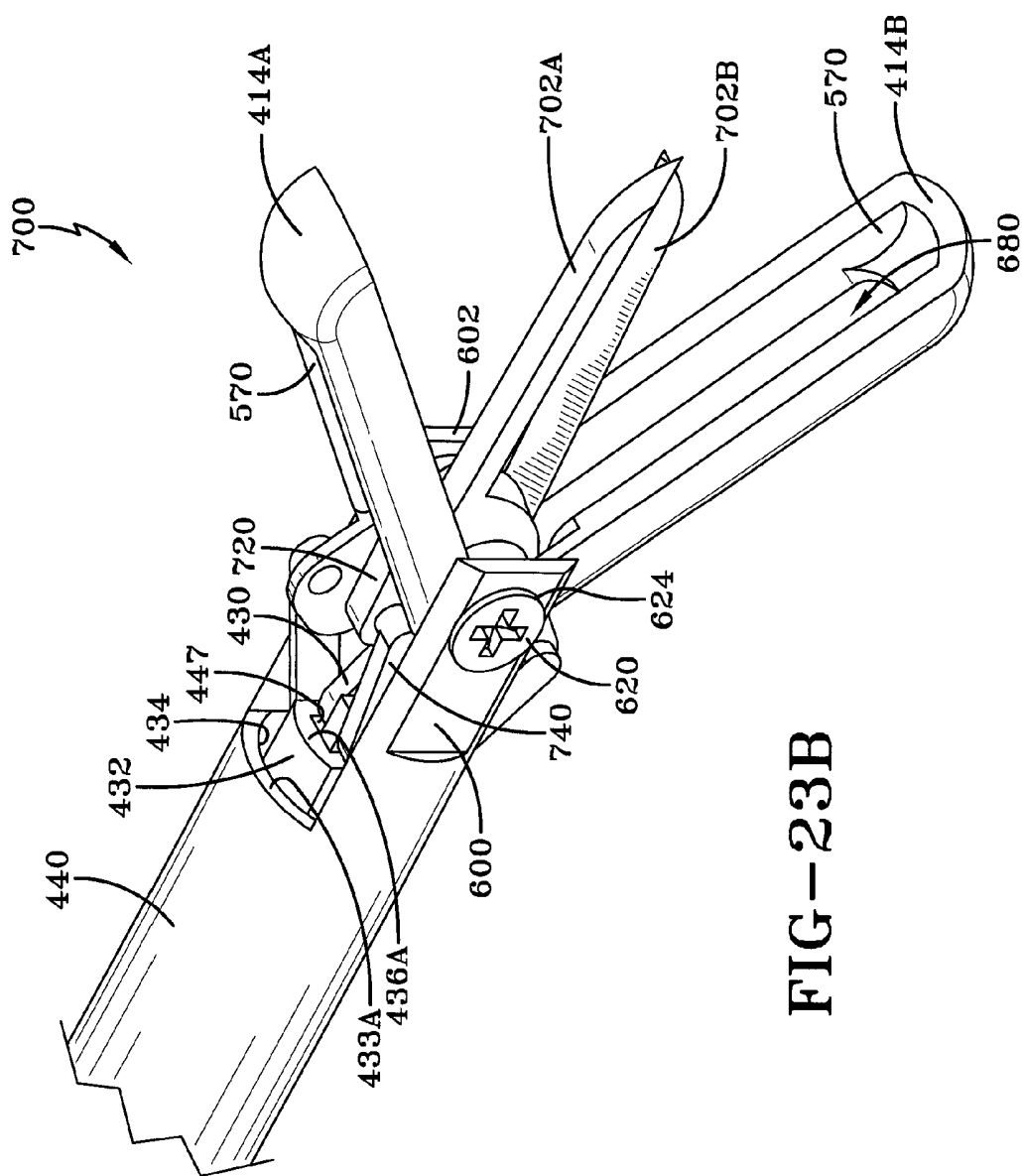


FIG-23A



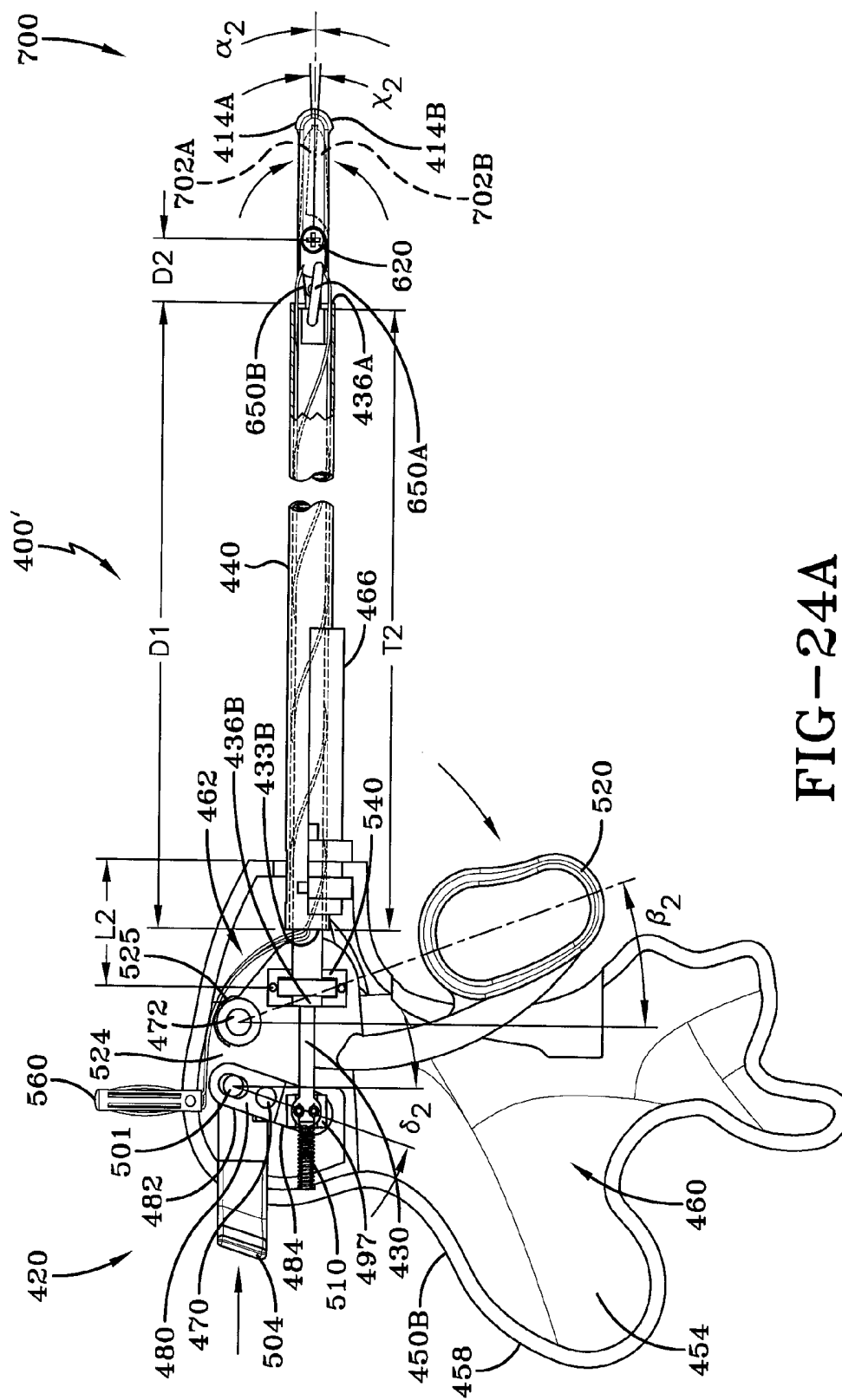


FIG-24A

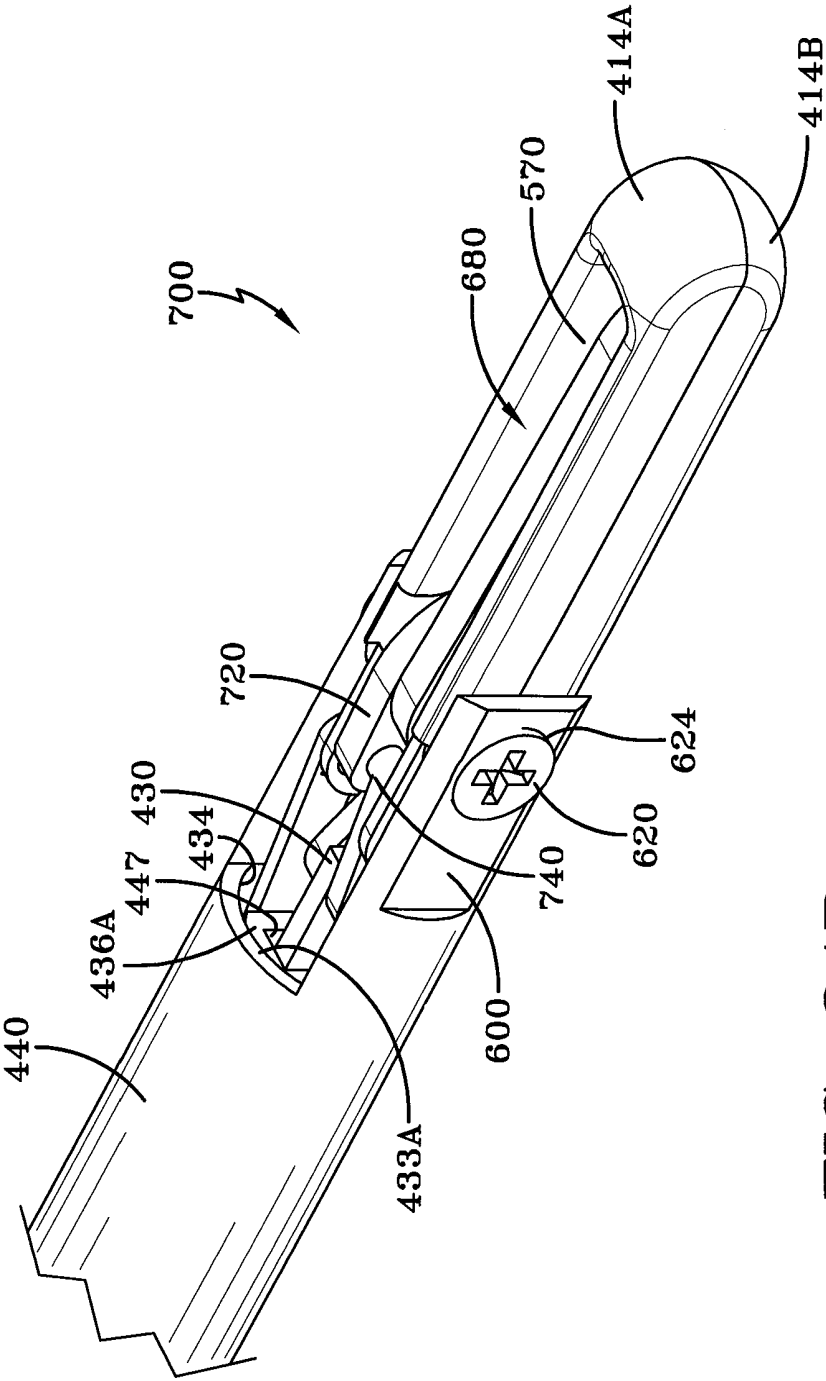
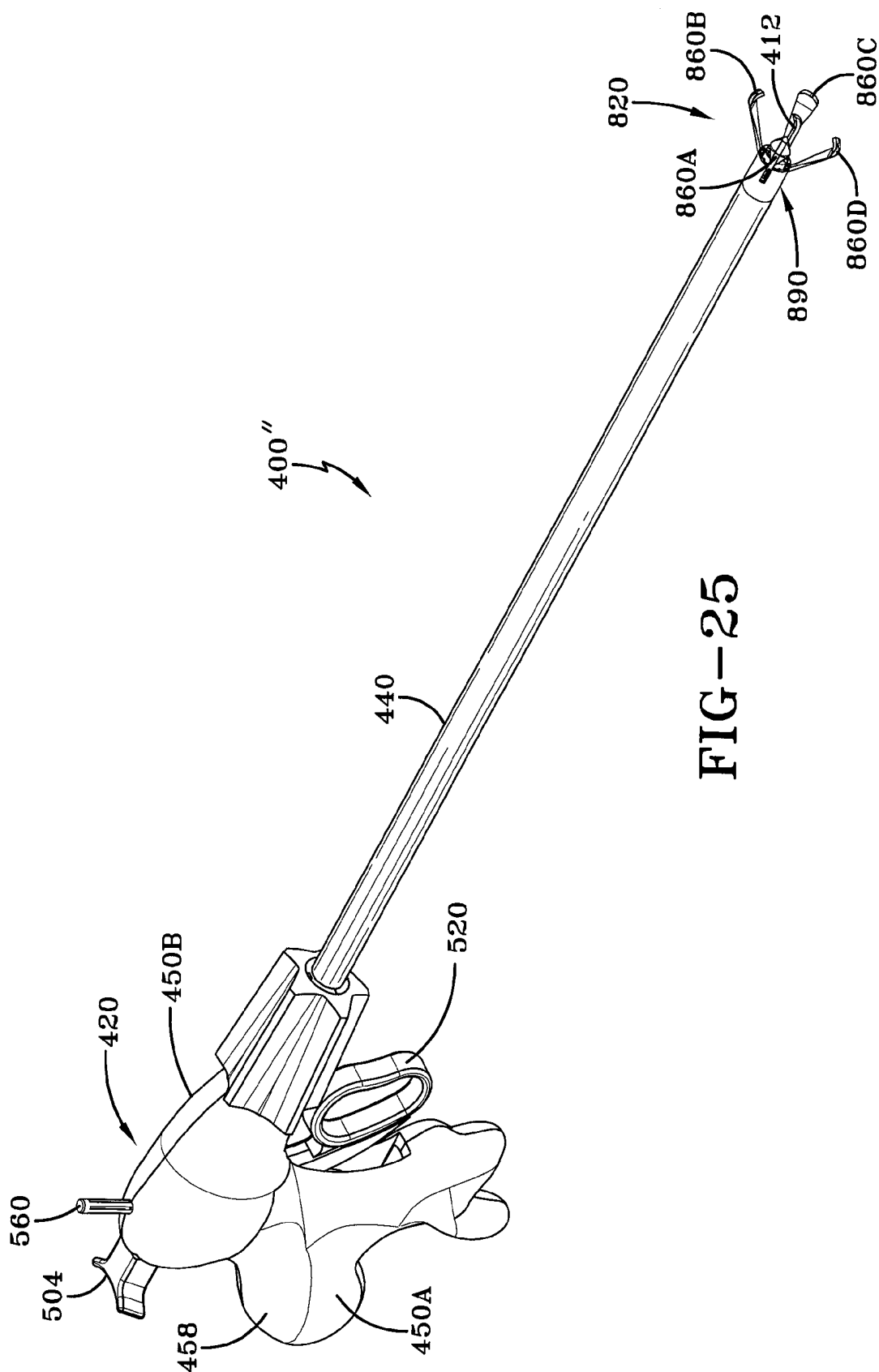
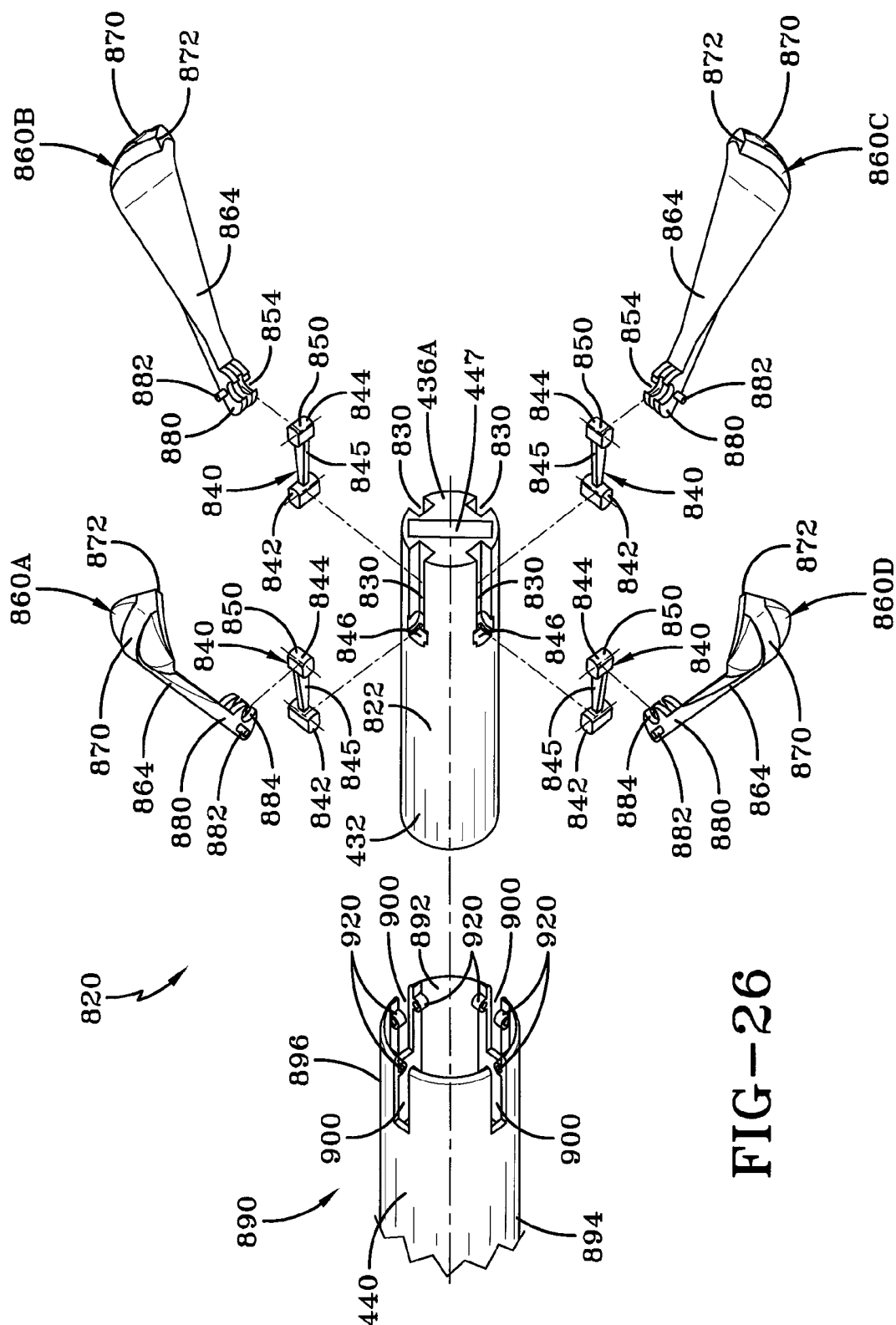
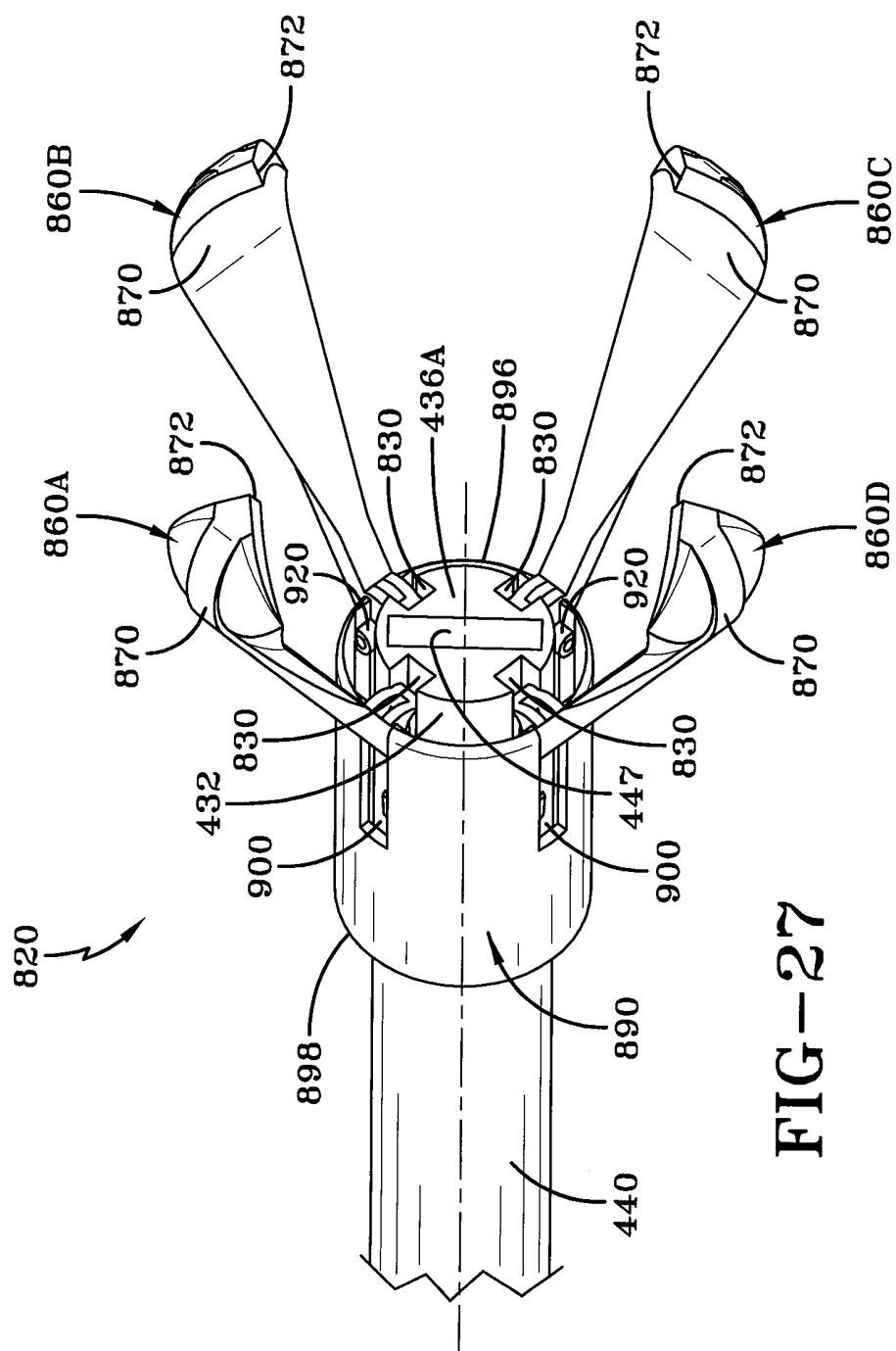
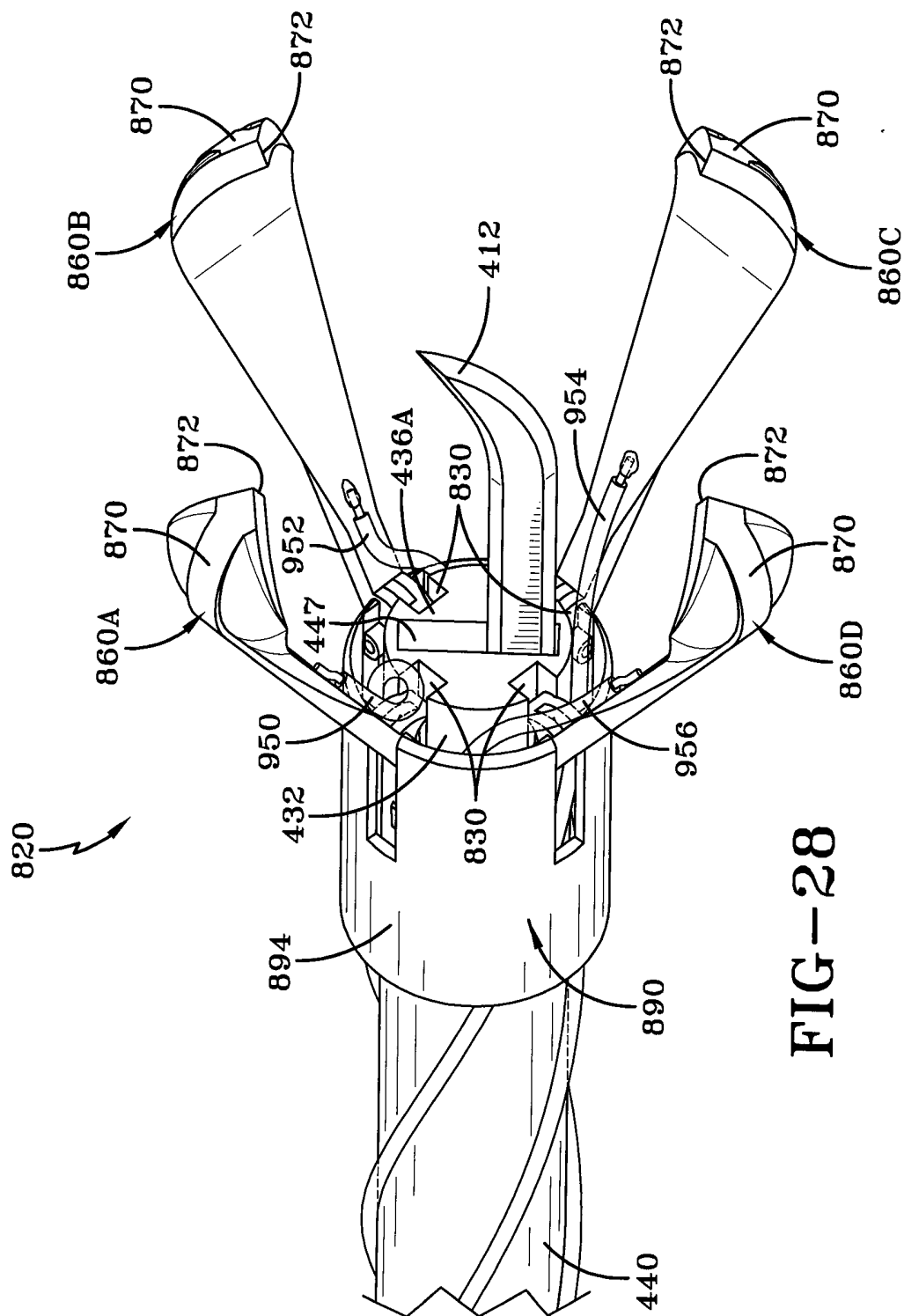


FIG-24B









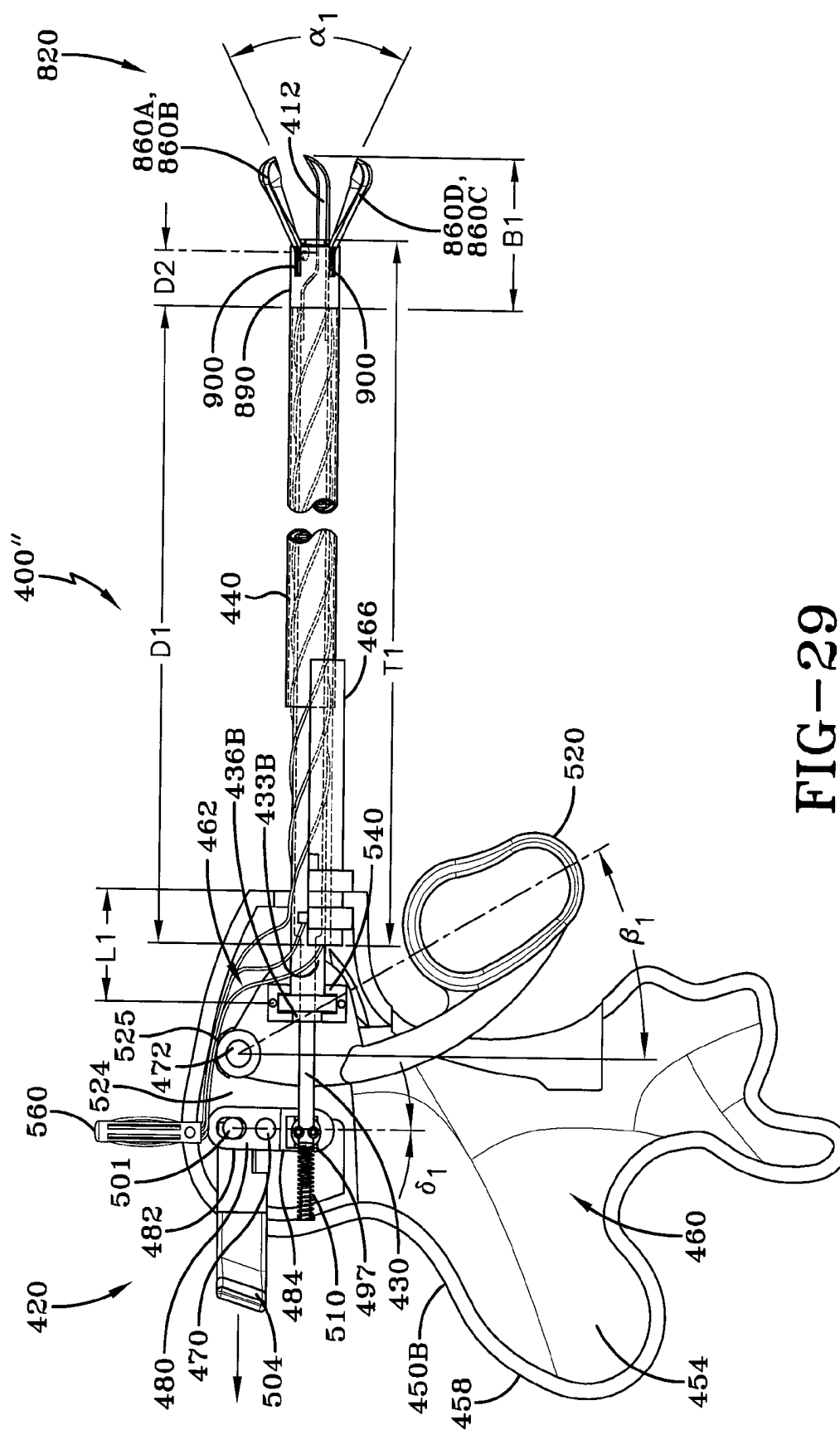


FIG-29

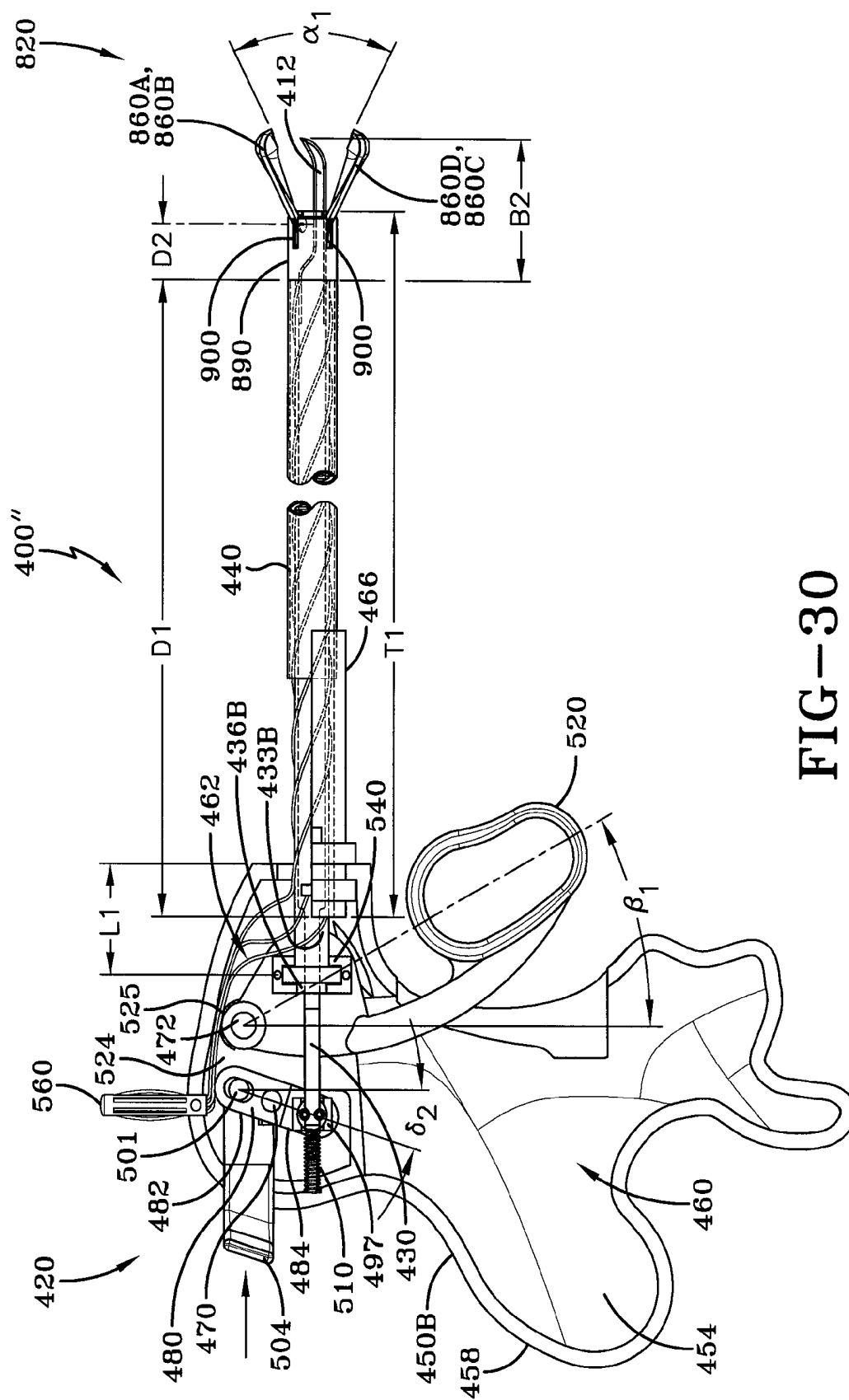
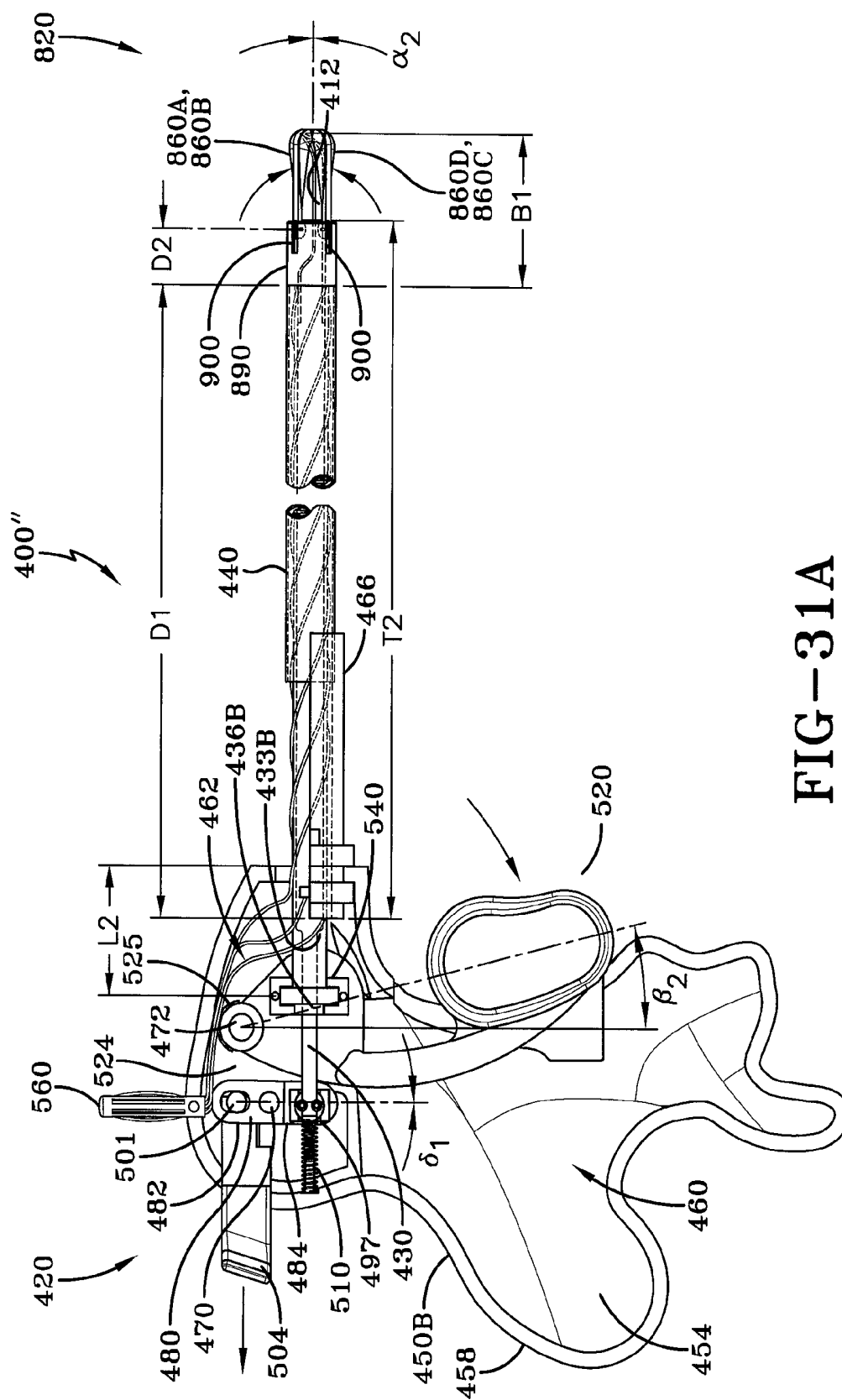


FIG-30



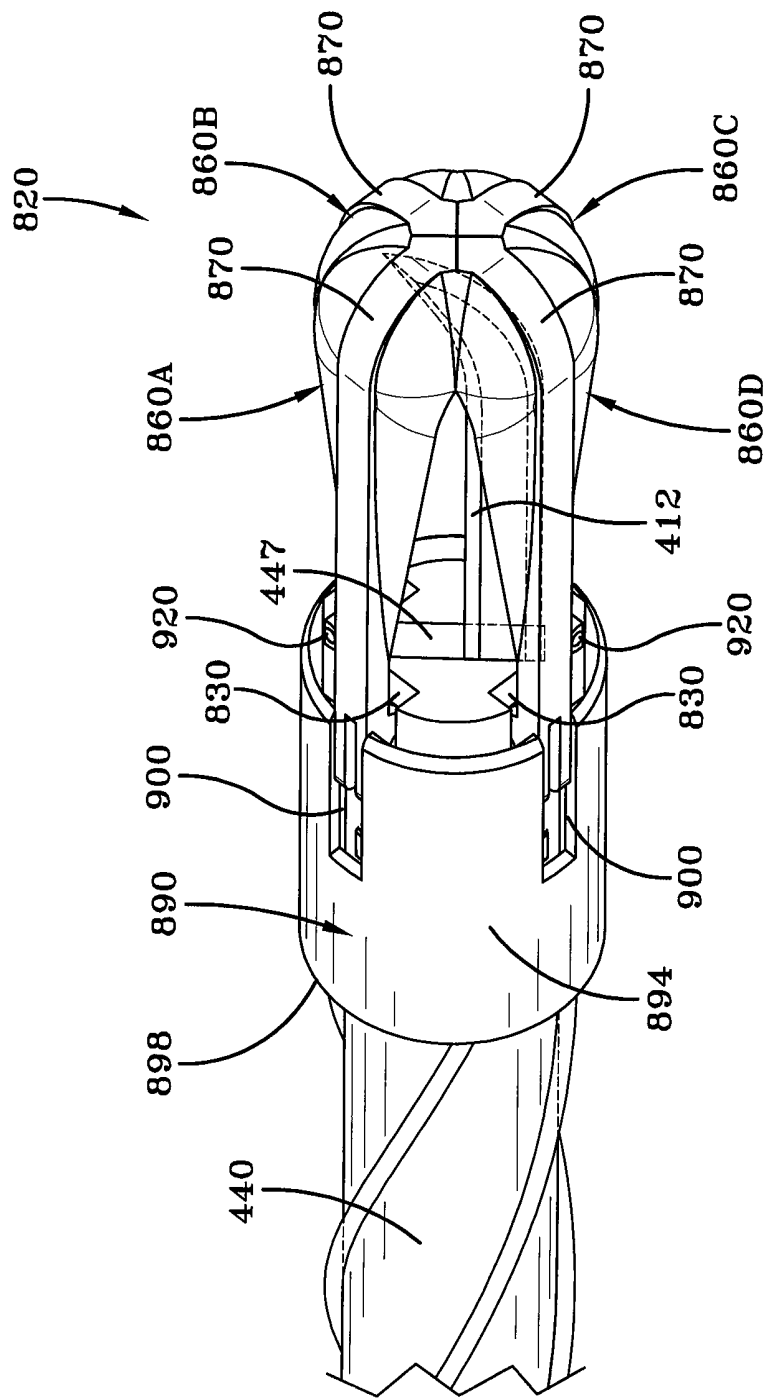


FIG-31B

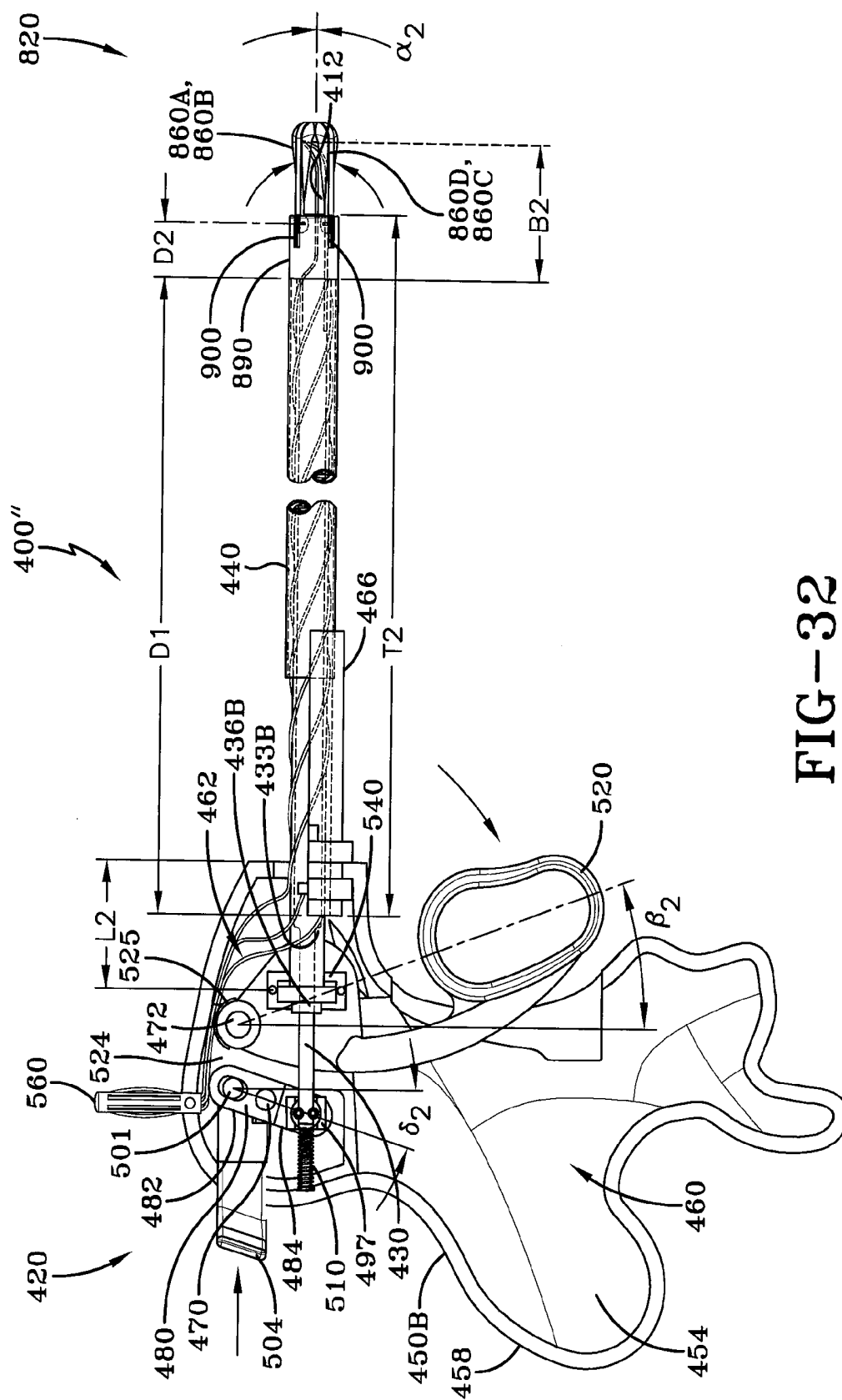


FIG-32

VARIABLE-FREQUENCY STIMULATOR FOR ELECTROSURGERY

TECHNICAL FIELD

[0001] Generally, the present invention relates to surgical devices used to perform electrosurgery. In particular, the present invention relates to a variable-frequency stimulator used to perform electrosurgery that optimizes the frequency of applied electrical current to reduce the electrical impedance of the biological tissue being treated. More particularly, the present invention relates to a variable-frequency stimulator and laparoscope configured to deliver electrical current to biological tissue at multiple contact points, to minimize the spread of electrical current through the tissue, so as to prevent collateral damage to tissue surrounding the surgical site.

BACKGROUND ART

[0002] Electrosurgery is a widely accepted technique and is used to perform a variety of manual or robot-assisted surgical procedures on biological tissue. For example, electrosurgery is used to hemostatically occlude blood vessels, as well as to perform tonsillectomies, vaginal hysterectomies, and amputation of the liver tip and splenic wedge, as well as to treat polycystic ovary syndrome, remove benign and malignant lesions of the skin, and to perform intradiscal electrothermal therapy for internal disc disruptions of the spine. However, surgeons that utilize currently available robotic and manual laparoscopic electrostimulation devices for electrosurgery are often unable to prevent collateral damage, such as the overheating, charring, and tearing, to the tissue surrounding the surgical site. Collateral damage is caused by the uncontrolled spread of energy from the electrostimulation device through tissue that is located in and about the surgical site. Furthermore, the rate of collateral damage caused by laparoscopic electrosurgical stimulators, due to the uncontrolled spread of electricity also tends to increase with repeated use of such electrosurgical devices. Unfortunately, such collateral damage often leads to surgical complications, increased pain and discomfort, and longer hospital stays, which increase the costs to the patient.

[0003] Although current commercially-available electrosurgical devices use a constant stimulation frequency that is between about 300 kHz to 3 MHz, for example, the biological tissue being treated by such devices has a conductivity that is dependent on the stimulation frequency used. For example, biological tissue, including kidney, liver, lung, heart, spleen, uterus, thyroid, testes, ovary, bladder, tongue, cartilage, muscle, and skin tissue all have an electrical conductivity that tends to increase with increasing stimulation frequencies. However, there are many other examples showing that the conductivity of these tissues can increase by more than two orders of magnitude over a frequency range from 10 Hz to 20 GHz. In addition, changes in electrical conductivity in biological tissue may also be caused by mechanical changes in the structure of biological tissue itself. For example, it has been shown that the electrical conductivity of porcine lung tissue has a large variation in depending on whether the lung is inflated or deflated, which is due to the significant mechanical changes of the structure of the lung during pneumoconstriction. Thus, a wide array of electrosurgical procedures can be positively impacted by providing a variable-frequency stimulator device that is able to deliver an adjustable stimulation frequency to increase the conductivity of the tissue being treated.

[0004] In addition, while electrosurgical techniques have improved due to various technological breakthroughs, including advancements in controlling the electrical current, clinically-relevant problems still exist with robotic and manual laparoscopic electrosurgical devices. Thus, surgeons still have difficulty avoiding collateral damage in and about the surgical site being treated by electrosurgical devices. As such, surgical complications from electrosurgery still frequently occur, which result in patient dissatisfaction and increased hospitalization costs, which are unwanted.

[0005] Therefore, there is a need for a variable-frequency stimulator for electrosurgery, which controls the conductivity of the biological tissue by varying a stimulation frequency. In addition, there is a need for a variable-frequency stimulator for electrosurgery that can be readily used with any commercially available robotic or manual electrosurgical device, such as a tissue dissector or laparoscope. There is also a need for a variable-frequency stimulator that provides improved electrosurgical efficacy and safety margins, and that reduces the occurrence of collateral damage to tissue surrounding the surgical site being treated. Moreover, there is a need for a laparoscope for use with a variable-frequency stimulator that is configured to concentrate the electrical current near the surface of the surgical site to prevent the uncontrolled spread of electrical current through the tissue, so as to reduce or prevent collateral damage to nearby tissue.

SUMMARY OF INVENTION

[0006] In light of the foregoing, it is a first aspect of the present invention to provide a variable-frequency stimulator for performing electrosurgery on tissue comprising a controller; a switch coupled to said controller, said switch configured to be placed into either of a first state or a second state; a surgical instrument coupled to said switch, said surgical instrument configured to contact the tissue; an impedance analyzer coupled to said controller and to said switch, said impedance analyzer configured to identify the impedance of tissue over a range of frequencies; and a frequency generator coupled to said controller and to said switch, said frequency generator configured to generate an electrical signal at a frequency greater than about 3 MHz, wherein when said switch is in said first state and said surgical instrument is in contact with the tissue, said impedance analyzer is electrically coupled to said surgical instrument to identify a frequency or range of frequencies in said frequency range that lowers the impedance and/or increases the conductivity of the tissue, and when said switch is in said second state, said frequency generator is coupled to said surgical instrument, so as to apply said electrical signal at said identified frequency or range of frequencies to the tissue.

[0007] It is another aspect of the present invention to provide a variable-frequency stimulator for performing electrosurgery on tissue comprising a controller; a switch coupled to said controller, said switch configured to be placed into either of a first state or a second state; a surgical instrument coupled to said switch, said surgical instrument configured to contact the tissue; an impedance analyzer coupled to said controller and to said switch, said impedance analyzer configured to identify the impedance of tissue over a range of frequencies; and a frequency generator coupled to said controller and to said switch, said frequency generator configured to generate an electrical signal; and wherein when said switch is in said first state and said surgical instrument is in contact with the tissue, said impedance analyzer is electrically coupled to said

surgical instrument to identify the lowest impedance of the tissue that is associated with said frequency range, said impedance analyzer also identifying a test impedance in the tissue at a predetermined test frequency, said controller calculating the ratio of said test impedance to the lowest impedance associated with said frequency range to set the power level output by the frequency generator, and when said switch is in said second state, said frequency generator is coupled to said surgical instrument, so as to apply said electrical signal having a frequency that is associated with the lowest impedance and/or highest conductivity to the tissue.

[0008] It is yet another aspect of the present invention to provide a method of performing electrosurgery on tissue comprising the steps of providing a frequency generator and an impedance analyzer that are coupled to a controller, said frequency generator generating an electrical signal at a frequency greater than about 3 MHz; providing a surgical instrument that is electrically coupled to said frequency generator and said impedance analyzer; contacting the tissue with said surgical instrument; identifying the impedance of the tissue with said impedance analyzer over a range of associated frequencies; identifying a set frequency that reduces the impedance and/or increases conductivity of the tissue; adjusting the frequency of said electrical signal generated by said frequency generator to said set frequency; and applying said electrical signal to the tissue via the surgical instrument.

[0009] It is a further aspect of the present invention to provide a method of performing electrosurgery on tissue comprising the steps of providing a frequency generator and an impedance analyzer that are coupled to a controller storing a predetermined set impedance, said frequency generator generating an electrical signal; providing a surgical instrument that is electrically coupled to said frequency generator and said impedance analyzer; contacting the tissue with said surgical instrument; identifying the impedance of the tissue with said impedance analyzer over a range of associated frequencies; adjusting the frequency of said electrical signal generated by said frequency generator to obtain said set impedance; and applying said electrical signal at said frequency to the tissue via the surgical instrument.

[0010] It is another aspect of the present invention to provide a laparoscope comprising a hand grip operatively carrying a thumb trigger and a hand trigger; an elongated support shaft extending from said hand grip; a first actuation member slideably disposed within said support shaft, said first actuation member having opposed first and second ends with a cavity extending therebetween, said first end of said first actuation member attached to said hand trigger; at least two electrically-isolated grasping arms carried by said body and operatively attached with said second end of said actuation member, said at least two grasping arms configured to move between opened and closed positions; a connection interface electrically coupled to said at least two electrically-isolated grasping arms, said connection interface adapted to be connected to the electrostimulator; a second actuation member slideably disposed within said cavity, said second actuation member having opposed first and second ends, said first end of said second actuation member attached to said thumb trigger; and a cutting blade attached to said second end of said second actuation member and said support shaft, said cutting blade extending at least partially between said at least two grasping arms.

[0011] Yet still another aspect of the present invention is to provide a laparoscope comprising a hand grip operatively

carrying a thumb trigger and a hand trigger; an elongated support shaft extending from said hand grip; a first actuation member slideably disposed within said support shaft, said first actuation member having opposed first and second ends with a cavity extending therebetween, said first end of said first actuation member attached to said hand trigger; at least two electrically-isolated grasping arms carried by said body and operatively attached with said second end of said actuation member, said at least two grasping arms configured to move between opened and closed positions; a connection interface electrically coupled to said at least two electrically-isolated grasping arms, said connection interface adapted to be connected to the electrostimulator; a second actuation member slideably disposed within said cavity, said second actuation member having opposed first and second ends, said first end of said second actuation member attached to said thumb trigger; and a scissor assembly attached to said second end of said second actuation member and said support shaft, said scissor assembly extending at least partially between said at least two grasping arms.

[0012] Another aspect of the present invention is to provide a variable-frequency stimulator for performing electrosurgery on tissue comprising a controller; a surgical instrument coupled to said controller and adapted to contact the tissue; and a frequency generator coupled to said controller and configured to supply an electrical signal to said surgical instrument, wherein when said frequency generator is coupled to said surgical instrument, so as to apply said electrical signal at a frequency greater than about 3 MHz to the tissue, thereby reducing the impedance and/or increasing the conductivity of the tissue.

BRIEF DESCRIPTION OF THE DRAWINGS

[0013] These and other features and advantages of the present invention will become better understood with regard to the following description, appended claims, and accompanying drawings wherein:

[0014] FIG. 1 is a block diagram of a variable-frequency stimulator in accordance with the concepts of the present invention; and

[0015] FIG. 2A is a perspective view of a fixture used to hold a plurality of thermocouples or thermistors in contact with the tissue surrounding a surgical site in accordance with the concepts of the present invention;

[0016] FIG. 2B is another perspective view of the fixture of FIG. 2A used to hold a plurality thermocouples in contact with the tissue surrounding the surgical site in accordance with the concepts of the present invention;

[0017] FIG. 3 is a schematic view of a four component Maxwell-Wagner tissue model;

[0018] FIG. 4 is a graph showing the response of the tissue model of FIG. 3 across impedance Z1;

[0019] FIG. 5 is a graph showing the response of the of the tissue model of FIG. 3 across impedance Z2;

[0020] FIG. 6 is a graph showing the input and output response of a 500 kHz stimulation frequency across impedance Z2 of the tissue model of FIG. 3, where the peak-to-peak voltage of the response is 1.0V;

[0021] FIG. 7 is a graph showing the input and output response of a 900 kHz stimulation frequency across the impedance Z2 of the tissue model of FIG. 3, where the peak-to-peak voltage of the response 2.0V;

[0022] FIG. 8 is a graph showing the input and output response of a 2 MHz stimulation frequency across the imped-

ance Z2 of the tissue model of FIG. 3, where the peak-to-peak voltage of the response is 2.6V;

[0023] FIG. 9 is graph showing the input and output response to a 610 kHz stimulation frequency across impedance Z2, where the peak-to-peak voltage of the response is 1.5V;

[0024] FIG. 10 is a graph showing the input and output response to a 400 kHz stimulation frequency across impedance Z2, where the peak-to-peak voltage of the response is 1.5V;

[0025] FIG. 11A is a graph showing the temperature measurements for liver tissue for 50 kHz and 30 MHz stimulation frequencies with a constant 15 W power setting;

[0026] FIG. 11B is a graph showing the temperature measurements for lung tissue for 500 kHz and 30 MHz stimulation frequencies with a constant 10 W power setting;

[0027] FIG. 11C is a graph showing the temperature measurements for muscle tissue for 500 kHz and 30 MHz stimulation frequencies with a constant 15 W power setting.

[0028] FIG. 12 is a perspective view of a laparoscope configured for use with the variable-frequency stimulator of FIG. 1 in accordance with the concepts of the present invention;

[0029] FIG. 13 is another perspective view of the laparoscope configured for use with the variable-frequency stimulator in accordance with the concepts of the present invention;

[0030] FIGS. 14A-D are perspective views of a hand grip provided by the laparoscope configured for use with the variable-frequency stimulator in accordance with the concepts of the present invention;

[0031] FIG. 15 is a partial exploded view of an end effector provided by the laparoscope configured for use with the variable-frequency stimulator in accordance with the concepts of the present invention;

[0032] FIG. 16 is a perspective view of the end effector provided by the laparoscope configured for use with the variable-frequency stimulator in accordance with the concepts of the present invention;

[0033] FIG. 17 is another perspective view of the end effector provided by the laparoscope configured for use with the variable-frequency stimulator in accordance with the concepts of the present invention;

[0034] FIGS. 18A-D are elevational views of the laparoscope configured for use with the variable-frequency stimulator showing the operation of the laparoscope when a thumb trigger and a hand trigger are actuated in accordance with the concepts of the present invention;

[0035] FIG. 19 is a perspective view of an alternative laparoscope configured for use with the variable-frequency stimulator in accordance with the concepts of the present invention;

[0036] FIG. 20A is a perspective view of a scissor assembly provided by the end effector of the alternative laparoscope configured for use with the variable-frequency stimulator in accordance with the concepts of the present invention;

[0037] FIG. 20B is a perspective view of the grasping arms provided by the end effector of the alternative laparoscope configured for use with the variable-frequency stimulator with the scissor assembly removed in accordance with the concepts of the present invention;

[0038] FIG. 21A is an elevational view of the grasping arms and scissor members of the alternative laparoscope configured for use with the variable-frequency stimulator in an opened position in accordance with the concepts of the present invention;

[0039] FIG. 21B is a perspective view of the grasping arms and scissor members of the alternative laparoscope configured for use with the variable-frequency stimulator in an opened position in accordance with the concepts of the present invention;

[0040] FIG. 22A is an elevational view of the alternative laparoscope configured for use with the variable-frequency stimulator, where the grasping arms are in a closed position and the scissor members are in an opened position in accordance with the concepts of the present invention;

[0041] FIG. 22B is a perspective view of the alternative laparoscope configured for use with the variable-frequency stimulator, whereby the grasping arms are in a closed position and the scissor members are in an opened position in accordance with the concepts of the present invention;

[0042] FIG. 23A is an elevational view of the alternative laparoscope configured for use with the variable-frequency stimulator, whereby the grasping arms are in an opened position and the scissor members are in a closed position in accordance with the concepts of the present invention;

[0043] FIG. 23B is a perspective view of the alternative laparoscope configured for use with the variable-frequency stimulator, whereby the grasping arms are in an opened position and the scissor members are in a closed position in accordance with the concepts of the present invention;

[0044] FIG. 24A is an elevational view of the alternative laparoscope configured for use with the variable-frequency stimulator, whereby the grasping arms and scissor members are in a closed position in accordance with the concepts of the present invention;

[0045] FIG. 24B is a perspective view of the alternative laparoscope configured for use with the variable-frequency stimulator, whereby the grasping arms and scissor members are in a closed position in accordance with the concepts of the present invention;

[0046] FIG. 25 is a perspective view of another alternative laparoscope having an alternative end effector configured for use with the variable-frequency stimulator in accordance with the concepts of the present invention;

[0047] FIG. 26 is an exploded view of the grasping arms provided by the alternative laparoscope configured for use with the variable-frequency stimulator in accordance with the concepts of the present invention;

[0048] FIG. 27 is a perspective view of the alternative laparoscope configured for use with the variable-frequency stimulator showing the grasping arms in an opened position in accordance with the concepts of the present invention;

[0049] FIG. 28 is a perspective view of the alternative laparoscope configured for use with the variable-frequency stimulator showing the grasping arms in an opened position in accordance with the concepts of the present invention;

[0050] FIG. 29 is an elevational view of the alternative laparoscope configured for use with the variable-frequency stimulator showing the grasping arms in an opened position in accordance with the concepts of the present invention;

[0051] FIG. 30 is an elevational view of the alternative laparoscope configured for use with the variable-frequency stimulator showing the grasping arms in an opened position in accordance with the concepts of the present invention;

[0052] FIG. 31A is an elevational view of the alternative laparoscope configured for use with the variable-frequency stimulator showing the grasping arms in a closed position in accordance with the concepts of the present invention;

[0053] FIG. 31B is a perspective view of the alternative laparoscope configured for use with the variable-frequency stimulator showing the grasping arms in a closed position in accordance with the concepts of the present invention; and

[0054] FIG. 32 is an elevational view of the alternative laparoscope configured for use with the variable-frequency stimulator showing the grasping arms in a closed position in accordance with the concepts of the present invention.

DETAILED DESCRIPTION OF THE INVENTION

[0055] A variable-frequency stimulator for electrosurgery is generally referred to by numeral **100**, as shown in FIG. 1 of the drawings. Specifically, the variable-frequency stimulator **100** includes a controller **110** that provides the necessary hardware and/or software to carry out the functions of the variable-frequency stimulator **100** to be discussed. Coupled to the controller **110** is a stimulation frequency generator **120**, which includes a voltage to frequency converter **130** that is coupled to an RF (radio frequency) amplifier **140**. The voltage to frequency converter **130** is configured to convert a voltage signal received from the controller **110** into a signal having a predetermined frequency. For example, the voltage to frequency converter **130** may be configured to generate electrical signals having a variable frequency, that a plurality of signals having different frequencies are generated over a frequency range. Alternatively, the frequency converter **130** may be configured to generate on signal at a fixed or discrete frequency, which does not vary over a range. For example, the voltage to frequency converter **130** may be configured to generate electrical signals at frequencies ranging between about 500 kHz to 250 MHz; ranging from about 3 MHz to 30 MHz, as well as ranging from about 500 kHz-20 GHz, although any other suitable frequency range may be used. Furthermore, it is contemplated that the voltage to frequency converter **130** may also be configured to generate electrical signals at a frequency range of any suitable increment or size. That is, the voltage to frequency converter **130** may generate signals over a range having a lower limit frequency of about 4 MHz to an upper limit frequency of any desired value (at any incremental divisions thereof), including but not limited to the upper limit frequencies of 5 MHz, 6 MHz, 7 MHz, 8 MHz, etc. . . . Furthermore, the signals generated by the voltage to frequency converter **130** having at a single frequency may utilize any desired frequency (at any incremental division thereof), such as frequencies of about 4 MHz and above for example. For example, frequencies of 5 MHz, 6 MHz, 7 MHz, 8 MHz, 9 MHz, etc. may be used. The RF amplifier **140**, also coupled to the controller **110**, is configured to increase the amplitude of the electrical signal generated by the voltage to frequency converter **130** to a level preprogrammed at the controller **110** or manually set via a setting button **142**. The electrical signal output by the RF amplifier **140** having the desired frequency and amplitude characteristics is delivered to a switch **175** that is electrically coupled to a surgical instrument suitable for performing electrosurgery, such as a surgical instrument **180**. The surgical instrument **180**, which will be discussed in detail below, is a mechanical device, such as a laparoscope or tissue dissector, for example, that is configured to perform various manipulations, including electrosurgical manipulations, to biologic tissue, including but not limited to grasping, cutting, and cauterizing the tissue **190**. It should be appreciated by those well practiced in the art that the frequency of stimulation need not be specified by a volt-

age to frequency converter, but that any suitable means can be used to specify the frequency of stimulation.

[0056] The variable-frequency stimulator **100** also in one exemplary embodiment also includes an impedance analyzer **200** that is coupled to the controller **110** and to the switch **175**. It should be appreciated that the switch **175** may comprise any suitable mechanical, electrical, or electromechanical switching device that is configured to electrically couple either the frequency generator **120** or the impedance analyzer **200** with the surgical instrument **180**. Specifically, the impedance analyzer **200** is configured to identify the impedance or electrical conductivity of the tissue **190** that is being treated by the surgical instrument **180**. As such, the impedance analyzer **200** is configured to generate a plurality of electrical signals each with a different frequency that are applied to the tissue **190** to identify the associated tissue **190** impedance. That is, the impedance analyzer **200** is configured to sweep through a range of frequencies that are applied to the tissue **190** when the instrument **180** is brought into contact with the tissue **190**, and each associated impedance measurement is recorded by the controller **110**. Furthermore, the impedance analyzer **200** is configured to monitor the impedance of the tissue **190** over any desired range of frequencies, including but not limited to a range of frequencies, such as from about 500 kHz to 250 MHz; 100 kHz to 250 MHz; 3 MHz to 30 MHz, as well as ranging from about 500 kHz-20 GHz, for example. The impedance data acquired by the impedance analyzer **200** is recorded or stored by controller **110** and is processed in a manner to be discussed to determine the particular stimulation frequency that is to be delivered from the stimulator **120** to the tissue **190** via the electrosurgical instrument **180**.

[0057] Because the electrical conductivity of the tissue **190** is highly anisotropic and decreases when coagulated, it is important to frequently analyze the impedance of the tissue **190** by the frequency analyzer **200**. Thus, by controlling the electrical impedance of the tissue **190** being treated by variable-frequency electrical stimulation, less collateral damage will be inadvertently imposed upon surrounding biological tissue **190** due to a reduction in operating temperature. This is because the power dissipated by conductive elements can be described by $P=VI=I^2Z=V^2/Z$, where P is power, V is voltage, I is electrical current, and Z is the impedance of the element.

[0058] The variable-frequency stimulator **100** may be powered by any suitable AC (Alternating Current) or DC (Direct Current) power source **202**, such as a battery or standard wall outlet that is coupled to the controller **110**. Furthermore, a mode-select or setting switch **204** may be coupled to the controller **110** to place the variable-frequency stimulator **100** into various operating states or modes to be discussed below.

[0059] In one aspect, the variable-frequency stimulator **100** may be configured such that the control algorithm utilized by the controller **110** is programmed in MATLAB/Simulink using a real-time Windows target kernel and a control loop sample frequency of 1 kHz. In addition, the controller **110** may include a PCI-6221 (National Instruments) data acquisition card used to sample tissue temperature, voltage, and electrical current data in a manner to be discussed. In one aspect, the PCI-6221 data acquisition card may have two analog voltage outputs, whereby the first output is sent to the voltage-to-frequency converter **130** that is used to convert the variable voltage command signal from MATLAB/Simulink into a variable frequency. The second analog output from the controller will be sent to the high-bandwidth voltage controlled variable gain amplifier that will be used to adjust the

gain of the signal sent to an RF amplifier **140** and then subsequently to the tissue grasped by the instrument **180**. In another aspect, the impedance analyzer **200** may comprise an **4294A** impedance analyzer, which is used to measure the electrical frequency response of the tissue **190** that is in contact with the electrosurgical instrument **180** over a broad frequency range, as previously discussed.

[0060] In addition, the variable-frequency stimulator **100** may also include a plurality of temperature sensors **220**, such as a thermocouple or thermistor, that is attached to the tissue **190** and that is configured to monitor the temperature of the tissue **180** that surrounds the surgical site in which the surgeon is using the electrosurgical instrument **180**. The temperature identified by the temperature sensor **220** is delivered to the controller **110** and/or to a display monitor **240**, such as an LCD (liquid crystal display), for example. By allowing the surgeon to monitor the temperature of the tissue **190** via the display **240**, he or she is able to determine whether tissue **190** that is near to the region that is being treated by the electrosurgical instrument **180** is exceeding a threshold temperature and is in danger of being damaged. In one aspect, the controller **110** may utilize the temperature of the tissue **190** in order to vary the duty cycle and/or the frequency of the electrical current signal that is generated by the frequency generator **120**. This allows the surgeon to have better control of the function of the electrical stimulation applied by the tissue dissector, in the case of coagulation or cutting of tissue for example. It is also contemplated that the output of the impedance analyzer **200** may be coupled to the monitor **240** as well, to allow the surgeon to view the impedance of the tissue **190** being treated.

[0061] In one aspect, the temperature sensor **220** used to measure the temperature of the tissue **190**, may comprise five FLUKE 5611A silicon-bead probe thermocouples **220** that are carried by a polycarbonate fixture **242**, as shown in FIGS. 2A-B, which includes a slot that is dimensioned to receive various end-effectors of the electrosurgical instruments **180**, including those discussed in detail below. Specifically, the thermocouples or temperature sensors **220** may be placed in the fixture **242** at a 1 mm distance around a mouth **244**, which is dimensioned to receive the surgical instrument **180** to measure the temperature distribution profile during the surgical procedures. The fixture **242** also includes a spring clip mechanism **246** that allows the thermocouple device **220** to be removeably clipped to the tissue **190**, such that when the tissue **190** is subsequently stimulated by the variable-frequency stimulator **100**, the nearby tissue temperature is measured by the five thermocouples **220**. It should also be appreciated by those well practiced in the art that the tissue temperature could be measured by any suitable sensor such as an infrared sensor.

[0062] Thus, with the components of the variable-frequency stimulator **100** set forth, the following discussion sets forth the operational steps carried out by the variable-frequency stimulator **100** during its operation. Initially, before the tissue **190** is grasped with the surgical instrument **180**, the switch **175** is placed in a first mode or state, where the impedance analyzer **200** is electrically coupled to the surgical instrument **180**. Specifically, the impedance measured by the impedance analyzer **200** across the grasping arms of the surgical instrument **180** before they contact the tissue **190** is infinite, and when the tissue **190** is brought into contact or grasped with the instrument **180** the impedance becomes finite and the impedance analyzer **120** sweeps through a pre-

determined range of frequencies, as previously discussed. In one aspect, the sweep time of the impedance analyzer **200** over the range of frequencies may be achieved in less than 100 ms, for example, although other sweep times may be used. The impedance analyzer **200** continues analyzing the impedance of the tissue **190** over the predetermined frequency range until the surgeon activates the electrical stimulation function of the stimulator **100** by placing the switch **175** into a second mode or state. Placing the switch **175** into the second mode or state disconnects the impedance analyzer **200** from the surgical instrument **180**, and connects the frequency generator **120** to the surgical instrument **180**, thereby allowing electrical signals at a range of frequencies to be delivered to the surgical site as previously discussed. The impedance of the tissue can be determined while the tissue is stimulated through the ratio of the measured voltage and current.

[0063] In another aspect, the variable-frequency stimulator **100** may be configured to be placed in various operating modes via the mode-select switch **204**. Specifically, in a first or normal mode, the variable-frequency stimulator **100** utilizes a control algorithm that is executed by the controller **110**, which is programmed to deliver electrical signals over a range of stimulation frequencies, as previously discussed, which have a constant average power that produces a lower or the lowest level of tissue impedance over a specific frequency band. This allows the electrosurgical instrument **180** to have a fast cutting time, while allowing the temperature of the tissue **190** to remain low thereby reducing burns and collateral damage to the tissue. Specifically in one aspect, the tissue impedance at a stimulation frequency of about 500 kHz is compared by the controller **110** to the lowest tissue impedance measured over an entire predetermined frequency range, such as from about 100 kHz to 4 MHz or from about 300 kHz to 250 MHz, as determined by the impedance analyzer **200**, as previously discussed. Next, the ratio of the tissue impedance at 500 kHz with respect to a lower or the lowest measured impedance is calculated by the controller **110** in order to reduce the power level of the electrical stimulation, which would be implemented at the frequency producing the lowest tissue impedance. The frequency of stimulation can also be chosen without use of an impedance analyzer to reduce tissue impedance or increase tissue conductivity based on the knowledge that tissue conductivity increases in general with increasing stimulation frequency, in particular with stimulation frequencies greater than 3 MHz. It should also be clear that the frequency of stimulation corresponding to a lower or the lowest level of tissue impedance can be used without any reduction in power. It should also be clear that after a stimulation frequency in the range of, for example, 3 MHz-20 GHz is used, a lower frequency of stimulation for example between 300 kHz-3 MHz could be subsequently used. It should also be clear that the frequency and/or duty cycle of stimulation can be adjusted based on tissue temperature feedback to produce lower or more desirable operating temperatures. This algorithm produces less collateral damage, necrosis and operating temperatures that are lower than that produced by currently available constant frequency stimulators that typically operate between 300 kHz and 3 MHz. The frequency of electrical stimulation that would most closely produce the desired tissue impedance or conductivity is then used with a constant average power stimulation mode each time the tissue **190** is subsequently grasped by the instrument **180**.

[0064] In a second operating mode selected by the mode-select switch **204**, the electrostimulator **100** maximizes the

conductivity of the tissue **190**, by selecting a stimulating frequency from the range of analyzed stimulation frequencies that achieves the a lower or the lowest tissue impedance as identified by the impedance analyzer **200**. That is, the controller **110** utilizes the stimulation frequency and associated impedance data that is collected by the impedance analyzer **200** to control the voltage to frequency converter **130** and RF amplifier **140** of the frequency generator **120**, so as to generate a stimulation frequency that is applied to the tissue **190** that reduces or minimizes the impedance or increases or maximizes the conductivity of the tissue **190**. The reduction and/or minimization in impedance and/or the increase and/or maximization of conductivity is with respect to the levels of impedance and/or conductivity that can be obtained with lower frequency levels between for example 300 kHz-3 MHz. As such, the present invention is capable of lowering or reducing the impedance with respect to the impedance levels that can be obtained by commercially available devices that operate between 300 kHz-3 MHz, which is highly desirable.

[0065] In a third operating mode selected by the mode-select switch **204**, the controller **110** is configured to control the stimulating frequency such that the impedance of the grasped tissue is the same regardless of the type of tissue **190** being treated by the instrument **180**. This normalized operation of the variable-frequency electrostimulator **100** allows the surgeon or other operator of the device to have a consistent level of cutting and/or cauterizing control across all types of tissue. This is in contrast to the electrostimulator **100** operating modes previously discussed, which may vary the stimulation frequency to provide a lower or the lowest impedance depending on the type of tissue **190** being treated. That is, by configuring the electrostimulator **100** to select the necessary frequency to achieve the same level of impedance and/or conductivity independent of the type of tissue **190** allows the surgeon to apply a consistent the ratio of current to voltage for any specific power setting used to treat the tissue **190**, regardless of the type of tissue or the way that the a specific type of tissue is grasped. This ensures that consistent tissue heating effects occur regardless of the tissue that is treated.

[0066] In a fourth operating mode, any number of components from FIG. **1** may be omitted and a single electrical signal having a constant or fixed frequency of stimulation, as previously discussed, can be applied to the tissue with or without any feedback controller. In this embodiment, the specific frequency of stimulation can be specified ahead of time anywhere between a range of any desired frequencies, such as for example 4 MHz-20 GHz. This can be done to reduce collateral damage, tissue temperature and burning during electrosurgery, because the tissue impedance decreases in general with increasing stimulation frequency. The tissue conductivity also increases in general with increasing stimulation frequency. These two factors significantly impact the ratio of voltage to current for any power level that is used to cut tissue which in turn impacts the tissue temperature, collateral damage and tissue burning. The reduction and/or minimization in impedance and/or the increase and/or maximization of conductivity is with respect to the levels of impedance and/or conductivity that can be obtained with lower frequency levels between for example 300 kHz-3 MHz.

[0067] Thus, because most biological tissue impedances decrease with increasing stimulation frequency, control over the tissue impedance is possible through the control of the stimulation frequency via the variable-frequency stimulator **100**. As such, the stimulator **100** is configured to stimulate

tissue with a frequency that reduces and/or minimizes the electrical impedance of the tissue. Hence, the stimulator **100** is also configured to stimulate tissue with a frequency that increases and/or maximizes the electrical conductivity of the tissue. Such reduction and/or minimization of the electrical impedance of biological tissue treated by the stimulator **100** is able to reduce the operating temperatures of surrounding tissue to prevent or reduce the amount of collateral damage and tissue necrosis that occurs during electrosurgical procedures. It should also be appreciated that the variable-frequency stimulator **100**, through control of the frequency of stimulation can also control the amount and/or rate of blood loss, tissue temperature, tissue cauterization, and tissue burning that occurs during electrosurgery, which is highly desirable.

[0068] Experimental

[0069] To evaluate the efficacy of the methods of electrical stimulation utilized by the electrostimulator **100**, a four component Maxwell-Wagner model of tissue **300**, as shown in FIG. **3** was experimentally evaluated with an electrosurgical stimulator, using an electrosurgical instrument comprising bipolar laparoscope forceps. The default stimulation frequency was set at a constant 500 kHz, while a power setting of 1 W was used. Two different combinations of resistor and capacitor values were chosen to show how the constant frequency affects the voltage across the tissue model **300**. As shown in FIG. **4**, the peak-to-peak voltage applied by the stimulator is roughly 0.6V for resistors and capacitors (R_1 - R_2 and C_1 - C_2) having an effective impedance of Z_1 . However, for different values of resistance and capacitance (R_1 - R_2 and C_1 - C_2) with an effective impedance of Z_2 , the peak-to-peak voltage stimulator increases to roughly 3.5V, as shown in FIG. **5**.

[0070] In the next evaluation, a function generator was used to stimulate the tissue model (Z_2) at three different frequencies to show the advantage of using a variable stimulation frequency to allow the effective impedance of the tissue to be lowered. As shown from the stimulation frequencies at 900 kHz and 2 MHz, the voltage across the tissue model **300** is much larger compared to the input voltage than at the 500 kHz stimulation frequency, as shown in FIGS. **6**, **7**, and **8**. Specifically, FIG. **6** shows the response of the voltage across impedance Z_2 with a stimulation frequency of 500 kHz; FIG. **7** shows the increased amplitude in the voltage across impedance Z_2 when the stimulation frequency was increased to 900 kHz, even though the input amplitude is the same; FIG. **8** shows the increased amplitude in the voltage across impedance Z_2 when the stimulation frequency is increased to 2 MHz. Thus, variation of the stimulation frequency changes the amplitude of the voltage applied across impedance Z_2 .

[0071] Thus, the results set forth above show that the same amount of electrical current can be driven through the biological tissue **190** with a lower voltage when a stimulation frequency is chosen to minimize and/or reduce the effective impedance of the tissue **190**. During electrosurgery, this results in lower operating temperatures, and therefore less collateral damage to surrounding tissue. Furthermore, the results above also show that for any specified electric power level, a plurality of different ratios of voltage to current can be achieved by choice of the frequency of stimulation to control the impedance of the biological tissue **190**. This is important because of the different tissue heating effects that occur with

different ratios of voltage and current. Specifically, the temperature increase in the tissue from electrical stimulation is described by Eq. 1, where

$$\Delta T = \frac{J^2 t}{\sigma C_p d},$$

where J is the electric current density, t is the amount of time the tissue is stimulated, σ is the electrical conductivity, C_p is the specific heat of the tissue, and d is the density of the tissue. [0072] Therefore, when the stimulation frequency is selected to increase and/or maximize the tissue conductivity, the amount of time to cut the tissue is reduced, and the temperature of the tissue 190 will increase if a constant power stimulation mode is utilized. However, if the cutting time and all other parameters, except a, remain constant, a lower tissue temperature increase is achieved.

[0073] In addition, during the third mode of operation of the electrostimulator 100, impedances Z1 and Z2 of the model 300 are each stimulated at different frequencies. In the first case, impedance Z1 is stimulated with a peak-to-peak input of 20V and a frequency of 610 kHz, which resulted in a response of 1.5V peak-to-peak, as shown in FIG. 9. Next, impedance Z2 was stimulated with the same peak-to-peak input of 20V, but at a frequency of 400 kHz, which also resulted in a response of 1.5V peak-to-peak, as shown in FIG. 10. Thus, by choosing the appropriate stimulation frequency, the tissue impedance can be changed so that the voltage/current ratio can be kept the same. Thus, the current density through the tissue will remain constant and the heating of the tissue 190 described by Eq. 1 will be the same regardless of the type of tissue that is stimulated.

[0074] In addition, FIGS. 11A-C show temperature measurements in liver, lung, and muscle tissue when stimulating frequencies of 500 kHz and 30 MHz are used, as well as the average temperature of the tissue and corresponding standard deviation. It should be noted that the 30 MHz stimulation frequency produces a lower average temperature, with all three types of tissue, as shown in the Figs. For example, FIG. 11A shows the temperature measurements for liver tissue for 500 kHz and 30 MHz stimulation frequencies with a constant 15 W power setting, whereby the 30 MHz stimulation frequency produces a lower average tissue temperature. FIG. 11B shows the temperature measurements for lung tissue for 500 kHz and 30 MHz stimulation frequencies with a constant 10 W power setting, whereby the 30 MHz stimulation frequency produces a lower average tissue temperature. Finally, FIG. 11C shows the temperature measurements for muscle tissue for 500 kHz and 30 MHz stimulation frequencies with a constant 15 W power setting, whereby the 30 MHz stimulation frequency produces a lower average tissue temperature. Thus, the 30 MHz stimulation frequency produced a 14%, 11%, and 15% lower average maximum tissue temperature in the respective liver, lung, and muscle tissue than the 500 kHz stimulation frequency produced.

[0075] Thus, with the discussion of the components and manner of operation of the variable-frequency stimulation device 100 set forth, the following discussion presents the various surgical instruments 180 that may be utilized with the stimulation device 100. Specifically, the surgical instrument 180 may comprise a laparoscope 400, as shown in FIGS. 12-18 of the drawings. Specifically, the laparoscope 400 comprises an end effector 410 having a cutter or cutting blade 412

and grasping arms 414A-B that are operatively attached to a hand grip 420 via actuation members 430 and 432 that extend through an elongated cavity 434 disposed in an elongated support shaft 440 having opposed ends 433A and 433B. Specifically, the actuation members 430 and 432 have respective opposed ends 434A-B and 436A-B, such that ends 434A, 436A are operatively attached to the end effector 410 (cutting blade 412 and grasping arms 414A-B) and ends 434B, 436B are operatively attached to the handgrip 420. The actuation member 432 slideably reciprocates within the cavity 434 of the support shaft 440, and includes an elongated receiving cavity 447 in which the actuation member 430 slideably reciprocates. That is, the actuation member 432 slideably reciprocates within the cavity 434 of the support shaft 440, while the actuation member 430 slideably reciprocates within the cavity 447 of the actuation member 432. Specifically, the hand grip 420, shown clearly in FIGS. 14A-D, is formed as a pair of opposed case sections 450A and 450B. The case sections 450A-B have an opposed inner surface 454 and outer surface 458, such that when the housing sections 450A-B are attached together, a cavity 460 is formed therein to carry an actuation assembly 462 that controls the operation of the end effector 410.

[0076] The hand grip 420 is attached to the support shaft 440 via a collar 466. In addition, the hand grip 420 also includes a pair of spaced pivot shafts 470 and 472 that extend from the inner surface 454 of the housing section 450B at a substantially right angle. A yoke member 480 is pivotably attached to pivot shaft 470 via mounting aperture 481. The yoke member 480 includes a pivot arm 482 that is attached to a pair of parallel spaced yoke arms 484 and 486, whereby a pivot aperture 490 is disposed in the pivot arm 482, and yoke apertures 494 are disposed in each yoke arm 484, 486. It should be appreciated that the yoke member 480 may be formed as a single section or formed from two sections, as shown in the Figs. In addition, the spaced yoke arms 484, 486 are configured to retain a clamp 497 that includes protrusions 488 that are received within the yoke apertures 494. The clamp 497 is attached to an end cap 498 that is attached at end 434B of the actuation member 430. In addition, a thumb trigger 504 is pivotably attached to the pivot aperture 490 of the yoke member 480 by a protrusion 501. Furthermore, the yoke member 480 is biased by a spring 510 that is disposed between the end cap 498 and the inner surface 454 of the rear of the hand grip 450B. Thus, when the thumb trigger 504 is depressed from its normal resting position, the spring 510 is compressed and the cutting blade 412 attached to end 434A of the actuation member 430 is retracted within the support shaft 440, and when the thumb trigger 504 is released, the spring 510 decompresses, causing the yoke member 480 to pivot, such that the cutter 412 extends to its normal position.

[0077] The actuation assembly 462 also includes a hand trigger 520, as shown clearly in FIGS. 14A-D, which include a pivot aperture 524 that receives the protrusion 472 extending from the inner surface 454 of the case 450B therein, so as to allow the hand trigger 500 to pivot. The hand trigger 520 also includes spaced plates 524 and 526, each of which includes a receiving aperture 530 therein. The receiving apertures 530 are configured to pivotably receive protrusions 534 therethrough, which extends from an actuator clamp 540. The actuator clamp 540 is configured to be attached to the end 436B of an actuation member 432 that extends through the support shaft 440.

[0078] Thus, when the hand trigger 520 is squeezed or pulled backward from its normal resting position, a back edge 550 of the hand trigger 520 engages the yoke members 480, causing the cutter 412 to retract and the spring 510 to compress and the cutting blade 412 to retract, and the grasping arms 414A-B attached to the end 436A of the actuation member 432 to close. And when the hand trigger 520 is released, the spring 510 decompresses, such that the cutting blade extends forward and the grasping arms 414A-B open. Thus, due to the configuration of the thumb trigger 504 and the hand trigger 520, the cutter 412 and the grasping arms 414A-B are able to operate independently of one another.

[0079] In addition, the hand grip 420 also includes an electrical connection interface 560, such as a plug or port that is configured to electrically selectively couple the laparoscope end effector 410 to the switch 175 of the electrosurgical device 100.

[0080] Continuing to FIGS. 15-17, the pair of elongated grasping arms 414A-B of the end effector 410 each includes elongated apertures 570, as well as a pivot aperture 610 and an actuation aperture 614. As such, the grasping arms 414A and 414B are pivotably attached to respective attachment arms 600 and 602 that extend from the end 433A of the support shaft 440 by a suitable fasteners 620, such as a screw, that are received through the corresponding pivot apertures 610 and threadably retained in a fastener aperture 624 of the corresponding attachment arm 600 and 602. That is, the grasping arm 414A is pivotably attached to attachment arm 600 and grasping arm 414B is pivotably attached to attachment arm 602. In addition, dielectric bushings 630 are disposed between each fastener 620 and the inner circumference of the fastener aperture 624, so as to electrically isolate each grasping arm 414A and 414B from each other. In addition, wires 626 and 628 are respectively coupled at one end to the grasping arms 414A-B, and at another end to the connection interface 560.

[0081] In order to move the grasping arms 414A-B from an opened position to a closed position, the actuation member 432 includes pivot apertures 670A-B that are disposed proximate to the end 436A. Specifically, the pivot apertures 670A-B of the actuation member 432 are attached to respective grasping arms 414A-B by corresponding linkage members 650A-B. That is, linkage member 650A is pivotably attached between pivot aperture 614 of grasping arm 414A and pivot aperture 670A of the actuation member 432, and linkage member 650B is pivotably attached between pivot aperture 614 of grasping arm 414B and pivot aperture 670B of the actuation member 432. As such, when the connection interface 560 is electrically coupled to the switch 175, the variable-frequency stimulator 100 is electrically coupled to the grasping arms 414A-B. Furthermore, to allow the grasping arms 414A-B to be electrically isolated from each other, the pivot apertures 670A-B of the actuation member 432 may be electrically isolated from the linkage arms 650A-B by dielectric bushings 630, or alternatively, the linkage arms 650A-B may be formed from non-conductive dielectric material.

[0082] The cutting blade or cutter 412 provided by the laparoscope 400 is attached to the end 434A of the actuation member 430. Specifically, the cutting blade 412 is configured to extend within a gap or cavity 680 formed between the grasping arms 414A-B, whereby they are closed. Furthermore, the actuation member 430 to which the cutter 412 is attached is disposed within the cavity 447 of the actuation

member 432 and is configured to reciprocate back and forth by the operation of the thumb trigger 504 of the hand grip 420 previously discussed.

[0083] Thus, when the laparoscope 400 is initially placed into use whereby neither the thumb trigger 504 nor the hand trigger 520 are actuated by the user, the cutting blade 412 is extended to its normal resting position, and the grasping arms 414A-B are maintained in an opened state, as shown in FIG. 18A. When the hand trigger 520 is squeezed and the thumb trigger 504 is left in its normal resting position, the grasping arms 414A-B are closed, and the cutting blade remains in its normal resting position, as shown in FIG. 18B. Alternatively, when the thumb trigger 504 is depressed and the hand trigger 520 is left in its normal position, as shown in FIG. 18C, the cutting blade 412 is partially or fully retracted. Finally, when both the thumb trigger 504 is depressed and the hand trigger 520 is squeezed, the cutting blade 412 is fully/partially retracted, and the grasping arms 414A-B are closed, as shown in FIG. 18D.

[0084] In another aspect of the present invention, an alternative laparoscope 400' may comprise a scissor assembly 700, as shown in FIGS. 19-24, which replaces the cutting blade 412 previously discussed, with regard to laparoscope 400 shown in FIGS. 12-18. That is, the end effector 410 of laparoscope 400' is structurally equivalent to that of laparoscope 400 except that the cutting blade 412 of laparoscope 400 has been replaced with the scissor assembly 700. Specifically, the scissor assembly 700 includes a pair of scissor members 702A-B, each having a pivot aperture 710 and an actuation aperture 720, as shown in FIGS. 20A-B. A shaft 722 is disposed between attachment arms 600, 602 and is received through the pivot apertures 710 of each scissor member 702A-B. In addition, linkage members 740 and 744 formed of dielectric material are pivotably attached to the actuation aperture 720 of each respective scissor member 702A-B at one end, and to pivot apertures 750 disposed on each side of the actuation member 430 at another end of the linkage members 740. In another aspect, the scissor members 702A and 702B may be separated by a dielectric or non-conductive washer (not shown), such that the scissor members 702A-B are electrically isolated from one another, so as to ensure that the grasping arms 414A-B remain electrically isolated from each other.

[0085] Thus, during operation of the laparoscope 400', when it is in its normal resting position and the thumb trigger 504 and hand trigger 520 are not actuated, the grasping arms 414A-B and scissor members 702A-B are opened, as shown in FIGS. 21A-B. When the hand trigger 520 is squeezed and the thumb trigger 504 is not depressed, the grasping arms 414A-B are closed, as shown in FIGS. 22A-B, and the scissor members 702A-B remain opened and extend through the elongated apertures 570 of the grasping arms 414A-B. Alternatively, when the thumb trigger 504 is depressed and the hand trigger 520 is not squeezed, the scissor members 702A-B are closed, while the grasping arms 414A-B are opened, as shown in FIGS. 23A-B. Finally, when the thumb trigger 504 is depressed and the hand trigger 520 is squeezed, the scissor members 702A-B and the grasping arms 414A-B are both closed, as shown in FIGS. 24A-B.

[0086] In another embodiment of the present invention a laparoscope 400", which is structurally equivalent to laparoscope 400, except that end effector 410 has been replaced with alternative end effector 820 is shown in FIGS. 25-32 of the drawings. Specifically, the end effector 820 is configured

such that a plurality of spaced notches **830** are disposed about an outer surface **822** of the actuation member **432**, proximate to the end **436A**, as shown in FIG.

[0087] **26.** The notches **830** are dimensioned to receive and retain corresponding pivot tabs **840** therein, which include a fastener end **842** that is attached to an opposed pivot end **844** by an extension member **845**. As such, the fastener end **842** of the pivot tab **840** is configured to be snap-fit or frictionally-fit into corresponding pivot holders **846** disposed in the notches **830** of the actuation member **432**, although any other suitable pivoting means of fixation or attachment may be used. The pivot end **844** of each pivot tab **840** includes a substantially cylindrical pivot surface **850** that is dimensioned to be pivotably attached within an arcuate pivot retainer **854** provided by each grasping arm **860A-D**. The grasping arms **860A-D** each include a support arm **864** that extends from the arcuate pivot retainer **854**, and which terminates at a curved claw **870**. In one aspect, the curved claw **870** of each of the grasping arms **860A-D** may terminate at a point or tip **872**. Finally, extending at a substantially right angle from either side of an outer surface **880** of the grasping arm **860A-D** at a point proximate to the pivot retainer **854** are pivot pins **882**.

[0088] The end effector **820** of the laparoscope **400"** also includes a substantially cylindrical collar member **890**, as shown in FIG. **27**, having an inner surface **892** and an outer surface **894**, and that is terminated at opposed ends **896** and **898**. The collar **890** includes a plurality of spaced notches **900** that are disposed proximate to the end **896** of the collar **890**, which are dimensioned to allow the support arm **864** of the respective grasping arms **860A-D** to slide therethrough. Furthermore, the collar **890** is dimensioned to receive the actuation member **432** therein, such that the notches **900** of the collar **890** are substantially aligned with the notches **830** of the actuation member **432**, thereby aligning the grasping arms **860A-D** to freely move through the collar notch **900**. In addition, the collar **890** also includes retention apertures **920** that are disposed on either side of the notch **900** that are dimensioned to receive the pivot pins **882** of each corresponding grasping arm **860A-D** therein.

[0089] Disposed within aperture **447** of the actuation member **432** is the actuation member **430** to which the cutting blade **412** is attached, as previously discussed with regard to the embodiment in FIGS. **12-18**.

[0090] In addition, because the laparoscope **400"** includes four grasping arms **860A-D**, four connection wires **950**, **952**, **954**, **956**, as shown in FIG. **28**, are used to connect each respective grasping arm **860A-D** to the connection interface **560**, such that suitable electric signals, as previously discussed, can be delivered to the grasping arms **860A-D**. Furthermore, it should be appreciated that collar **890** and actuation member **432** are electrically isolated from the grasping arms **860A-D** using known means, such that the grasping arms **860A-D** are each electrically isolated from each other. Furthermore, in one aspect, the grasping arms **860A-D** may be configured, such that arms **860A** and **860C** comprise positive terminals or electrodes and arms **860B** and **860D** comprise negative terminals or electrodes, however, it should be appreciated that the grasping arms **860A-D** may be configured to be positive or negative in any desired configuration. As such, electrical signal supplied by the frequency generator **120** of the variable-frequency stimulator **100** is able to flow in multiple paths between the various positive and negative terminals or electrodes of formed by the grasping arms **860A-D**, which serves to concentrate the flow of electrical current

through tissue being grasped by the grasping arms **860A-D**. Moreover, by concentrating the flow electrical current, collateral damage, such as overheating, charring, and burning is minimized or prevented. Furthermore, more precise tissue dissection is also enabled with more concentrated current flow.

[0091] Thus, during operation of the laparoscope **400"**, when the laparoscope **400"** is at its normal resting state, whereby the thumb trigger **504** and the hand trigger **520** are not actuated, the grasping arms **860A-D** are fully opened, and the cutting blade **412** is fully extended as shown in FIG. **29**. When the thumb trigger **504** is depressed, and the hand trigger **520** is not squeezed, the cutting blade **412** is partially or fully retracted into the cavity **447** of the actuation member **432**, and the grasping arms **860A-D** are fully opened, as shown in FIG. **30**. Alternatively, when the hand trigger **520** is squeezed, and the thumb trigger **504** is not depressed, the grasping arms **560A-D** are closed and the cutting blade **412** is extended, as shown in FIGS. **31A** and **31B**. Finally, when the thumb trigger **504** is depressed and the hand trigger **520** is squeezed, the cutting blade **412** is partially or fully retracted into the cavity **447** of the actuation member **432** and the grasping arms **860A-D** are closed, as shown in FIG. **32**. Thus, the reciprocating back and forth movement of the cutting blade **412** and the opening and closing of the grasping arms **860A-D** can be independently controlled by the thumb trigger **504** and the hand trigger **520**.

[0092] It will, therefore, be appreciated that one advantage of the present invention is that a variable-frequency stimulator for electrosurgery reduces overheating, charring, and tearing of tissue. Another advantage of the present invention is that the variable-frequency stimulator for electrosurgery utilizes a stimulation signal having a constant power. Still another advantage of the present invention is that the variable-frequency stimulator for electrosurgery allows a constant amount of power to be applied independently of the type of tissue being treated. An additional advantage of the present invention is that the variable-frequency stimulator provides a laparoscope that includes multiple grasping arms that permit electrical current to flow in multiple paths between the arms, so as to reduce the temperature of the tissue surrounding the surgical site. Yet another advantage of the present invention is that the variable-frequency stimulator for electrosurgery allows for improved electrosurgery efficacy and safety margins to be attained for not only robotic-assisted applications, such as cholecystectomy, fundoplications, gastric banding, hysterectomy, prostatectomy, and colectomy, but will also enable surgeons to expand the scope of the surgical procedures that are performed and enhance advanced procedures, such as esophagectomy, gastrojejunostomy, thymectomy, thoracic parasympathectomy, lobectomy, mediastinal parathyroidectomy and left pancreatic resection, for example. Still another advantage of the present invention is that a laparoscope for use with a variable-frequency stimulator for electrosurgery allows electrical current to be distributed through the tissue being treated at multiple sites, so as to allow the electrical current to be concentrated in a more localized manner to reduce heating and excessive damage of the tissue surrounding the treatment site.

[0093] Thus, it can be seen that the objects of the invention have been satisfied by the structure and its method for use presented above. While in accordance with the Patent Statutes, only the best mode and preferred embodiment has been presented and described in detail, it is to be understood that

the invention is not limited thereto or thereby. Accordingly, for an appreciation of the true scope and breadth of the invention, reference should be made to the following claims.

1. A variable-frequency stimulator for performing electrosurgery on tissue comprising:

- a controller;
- a switch coupled to said controller, said switch configured to be placed into either of a first state or a second state;
- a surgical instrument coupled to said switch, said surgical instrument configured to contact the tissue;
- an impedance analyzer coupled to said controller and to said switch, said impedance analyzer configured to identify the impedance of tissue over a range of frequencies; and
- a frequency generator coupled to said controller and to said switch, said frequency generator configured to generate an electrical signal at a frequency greater than about 3 MHz;

wherein when said switch is in said first state and said surgical instrument is in contact with the tissue, said impedance analyzer is electrically coupled to said surgical instrument to identify a frequency or range of frequencies in said frequency range that lowers the impedance and/or increases the conductivity of the tissue, and when said switch is in said second state, said frequency generator is coupled to said surgical instrument, so as to apply said electrical signal at said identified frequency or range of frequencies to the tissue.

2. The variable-frequency stimulator of claim 1, further comprising a display coupled to said controller, which indicates the impedance and/or conductivity of the tissue being treated.

3. The variable-frequency stimulator of claim 1, wherein said surgical instrument comprises a laparoscope.

4. The variable-frequency stimulator of claim 3, wherein said laparoscope includes at least two electrically-isolated grasping arms, so as to allow the electrical signal to flow through multiple contact points in the tissue when said laparoscope is in contact therewith.

5. The variable-frequency stimulator of claim 3, wherein said laparoscope includes at least four electrically-isolated grasping arms, so as to allow the electrical signal to flow through multiple contact points in the tissue when said laparoscope is in contact therewith.

6. The variable-frequency stimulator of claim 1, wherein said controller is configured to adjust the frequency of said electrical signal generated by said frequency generator, so that the impedance and/or conductivity of the tissue measured by said impedance analyzer is set at a specific impedance and/or conductivity value independently of the type of tissue in contact with the surgical instrument.

7. The variable-frequency stimulator of claim 6, further comprising a setting switch coupled to said controller to set said predetermined impedance value stored at said controller.

8. The variable-frequency stimulator of claim 1, further comprising:

- a plurality of temperature sensors coupled to said controller, said temperature sensors adapted to measure the temperature of the tissue.

9. The variable-frequency stimulator of claim 8, further comprising:

- a display coupled to said controller, said display configured to display the temperature measured by said temperature sensors.

10. The variable-frequency stimulator of claim 1, wherein said electrical signal applied by said surgical instrument said frequency generator controls the amount and/or rate of blood loss, tissue temperature, tissue cauterization, or tissue burning that occurs during electrosurgery.

11. The variable-frequency stimulator of claim 8, wherein said plurality of temperature sensors are carried by a fixture having a spring biased clip adapted to be removably attached to the tissue.

12. The variable-frequency stimulator of claim 8, wherein said controller monitors the temperature measured by said plurality of temperature sensors and adjusts the power level and/or duty cycle and/or frequency of the electrical signal generated by said frequency generator based on the temperature.

13. The variable-frequency stimulator of claim 1, wherein said electrical signal generated by said frequency generator delivers constant average power.

14. A variable-frequency stimulator for performing electrosurgery on tissue comprising:

- a controller;
- a switch coupled to said controller, said switch configured to be placed into either of a first state or a second state;
- a surgical instrument coupled to said switch, said surgical instrument configured to contact the tissue;
- an impedance analyzer coupled to said controller and to said switch, said impedance analyzer configured to identify the impedance of tissue over a range of frequencies; and
- a frequency generator coupled to said controller and to said switch, said frequency generator configured to generate an electrical signal;

wherein when said switch is in said first state and said surgical instrument is in contact with the tissue, said impedance analyzer is electrically coupled to said surgical instrument to identify the lowest impedance of the tissue that is associated with said frequency range, said impedance analyzer also identifying a test impedance in the tissue at a predetermined test frequency, said controller calculating the ratio of said test impedance to the lowest impedance associated with said frequency range to set the power level output by the frequency generator, and when said switch is in said second state, said frequency generator is coupled to said surgical instrument, so as to apply said electrical signal having a frequency that is associated with the lowest impedance and/or highest conductivity to the tissue.

15. A method of performing electrosurgery on tissue comprising the steps of:

- providing a frequency generator and an impedance analyzer that are coupled to a controller, said frequency generator generating an electrical signal at a frequency greater than about 3 MHz;
- providing a surgical instrument that is electrically coupled to said frequency generator and said impedance analyzer;
- contacting the tissue with said surgical instrument;
- identifying the impedance of the tissue with said impedance analyzer over a range of associated frequencies;
- identifying a set frequency that reduces the impedance and/or increases conductivity of the tissue;
- adjusting the frequency of said electrical signal generated by said frequency generator to said set frequency; and

applying said electrical signal to the tissue via the surgical instrument.

16. The method of claim **15**, further comprising:

adjusting the power level of said electrical signal based on the ratio of the impedance of the tissue at a predetermined frequency and a reduced tissue impedance and/or increased tissue conductivity that is associated with said range of frequencies.

17. The method of performing electrosurgery of claim **15**, further comprising the steps of:

providing a plurality of temperature sensors coupled to said controller;

attaching said temperature sensors to the tissue about the surgical site;

identifying the temperature of the tissue; and

adjusting the power level and/or duty cycle and/or frequency of said electrical signal based on the identified temperature.

18. A method of performing electrosurgery on tissue comprising the steps of:

providing a frequency generator and an impedance analyzer that are coupled to a controller storing a predetermined set impedance, said frequency generator generating an electrical signal;

providing a surgical instrument that is electrically coupled to said frequency generator and said impedance analyzer;

contacting the tissue with said surgical instrument;

identifying the impedance of the tissue with said impedance analyzer over a range of associated frequencies;

adjusting the frequency of said electrical signal generated by said frequency generator to obtain said set impedance; and

applying said electrical signal at said frequency to the tissue via the surgical instrument.

19. A laparoscope comprising:

a hand grip operatively carrying a thumb trigger and a hand trigger;

an elongated support shaft extending from said hand grip;

a first actuation member slideably disposed within said support shaft, said first actuation member having opposed first and second ends with a cavity extending therebetween, said first end of said first actuation member attached to said hand trigger;

at least two electrically-isolated grasping arms carried by said body and operatively attached with said second end of said actuation member, said at least two grasping arms configured to move between opened and closed positions;

a connection interface electrically coupled to said at least two electrically-isolated grasping arms, said connection interface adapted to be connected to the electrostimulator;

a second actuation member slideably disposed within said cavity, said second actuation member having opposed first and second ends, said first end of said second actuation member attached to said thumb trigger; and

a cutting blade attached to said second end of said second actuation member and said support shaft, said cutting blade extending at least partially between said at least two grasping arms.

20. The laparoscope of claim **19**, wherein said at least two grasping arms include apertures.

21. A laparoscope comprising:

a hand grip operatively carrying a thumb trigger and a hand trigger;

an elongated support shaft extending from said hand grip;

a first actuation member slideably disposed within said support shaft, said first actuation member having opposed first and second ends with a cavity extending therebetween, said first end of said first actuation member attached to said hand trigger;

at least two electrically-isolated grasping arms carried by said body and operatively attached with said second end of said actuation member, said at least two grasping arms configured to move between opened and closed positions;

a connection interface electrically coupled to said at least two electrically-isolated grasping arms, said connection interface adapted to be connected to the electrostimulator;

a second actuation member slideably disposed within said cavity, said second actuation member having opposed first and second ends, said first end of said second actuation member attached to said thumb trigger; and

a scissor assembly attached to said second end of said second actuation member and said support shaft, said scissor assembly extending at least partially between said at least two grasping arms.

22. The laparoscope of claim **21**, wherein said at least two grasping arms include apertures.

23. A variable-frequency stimulator for performing electrosurgery on tissue comprising:

a controller;

a surgical instrument coupled to said controller and adapted to contact the tissue; and

a frequency generator coupled to said controller and configured to supply an electrical signal to said surgical instrument;

wherein when said frequency generator is coupled to said surgical instrument, so as to apply said electrical signal at a frequency greater than about 3 MHz to the tissue, thereby reducing the impedance and/or increasing the conductivity of the tissue.

24. The variable-frequency stimulator of claim **23**, wherein said surgical instrument comprises a laparoscope.

25. The variable-frequency stimulator of claim **24**, wherein said laparoscope includes at least two electrically-isolated grasping arms, so as to allow the electrical signal to flow through multiple contact points in the tissue when said laparoscope is in contact therewith.

26. The variable-frequency stimulator of claim **24**, wherein said laparoscope includes at least four electrically-isolated grasping arms, so as to allow the electrical signal to flow through multiple contact points in the tissue when said laparoscope is in contact therewith.

27. The variable-frequency stimulator of claim **23**, further comprising:

a plurality of temperature sensors coupled to said controller, said temperature sensors configured to measure the temperature of the tissue.

28. The variable-frequency stimulator of claim **27**, further comprising:

a display coupled to said controller, said display configured to display the temperature measured by said temperature sensors.

29. The variable-frequency stimulator of claim **27**, wherein said plurality of temperature sensors are carried by a fixture having a spring biased clip adapted to be removably attached to the tissue.

30. The variable-frequency stimulator of claim **27**, wherein said controller monitors the temperature measured by said plurality of temperature sensors and adjusts the power level and/or duty cycle and/or frequency of the electrical signal generated by said frequency generator based on the temperature.

31. The variable-frequency stimulator of claim **23**, wherein said electrical signal generated by said frequency generator delivers constant average power.

32. The variable-frequency stimulator of claim **23**, further comprising a setting switch coupled to said controller, said setting switch configured to adjust the frequency of said electrical signal, so as to change the impedance of the tissue.

33. The variable-frequency stimulator of claim **23**, further comprising a display coupled to said controller, which indicates the impedance and/or conductivity of the tissue being treated.

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专利名称(译)	用于电外科的可变频率刺激器		
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当前申请(专利权)人(译)	阿克伦大学 SUMMA健康		
[标]发明人	ENGBERG ERIK ESPINAL ERIC		
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摘要(译)

用于电外科的可变频率刺激器包括阻抗分析器，用于识别由电外科器械（例如腹腔镜）治疗的生物组织的电阻抗。基于所识别的组织阻抗，控制器调节输送到电外科器械的电流的频率，以减小，最小化或标准化组织的阻抗，从而防止对手术部位内和周围的组织的附带损害。另外，腹腔镜可以配置有多个导电抓握臂，其用于将电流输送到手术部位。导电抓握臂为电流提供多个电流路径，从而在电外科手术过程中将电流集中在手术部位。因此，防止了组织中不希望的电流扩散，从而减少或防止对手术部位内和周围组织的附带损害。

