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(54) **CONNECTOR FOR A LAPAROSCOPIC
SURGICAL SYSTEM**

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(2013.01); **A61B 2017/2931** (2013.01); **A61B**
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(2013.01)

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2019/4873

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Primary Examiner — Gary Jackson

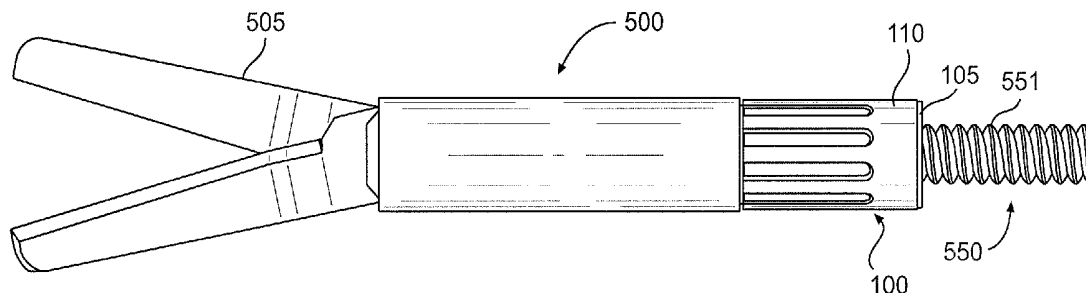
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(57) **ABSTRACT**

A connector for connecting an instrument tip with a laparo-
scopic tube end, the connector including a base forming a
body of the connector, the base having a lumen configured to
accommodate an instrument tip actuator therein, and a seal
permanently bonded to an inner surface of a proximal end of
the base and configured to deform upon connection of the
connector with the tube end.

33 Claims, 8 Drawing Sheets



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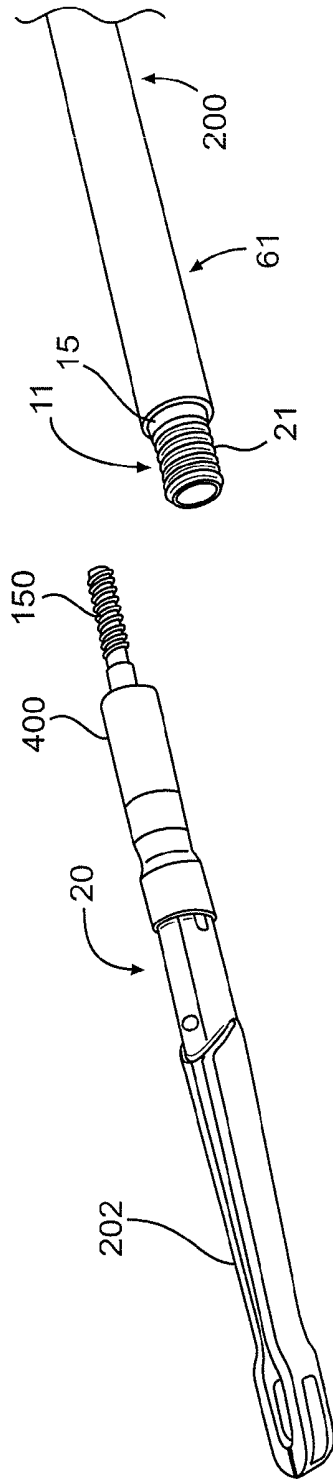


FIG. 1

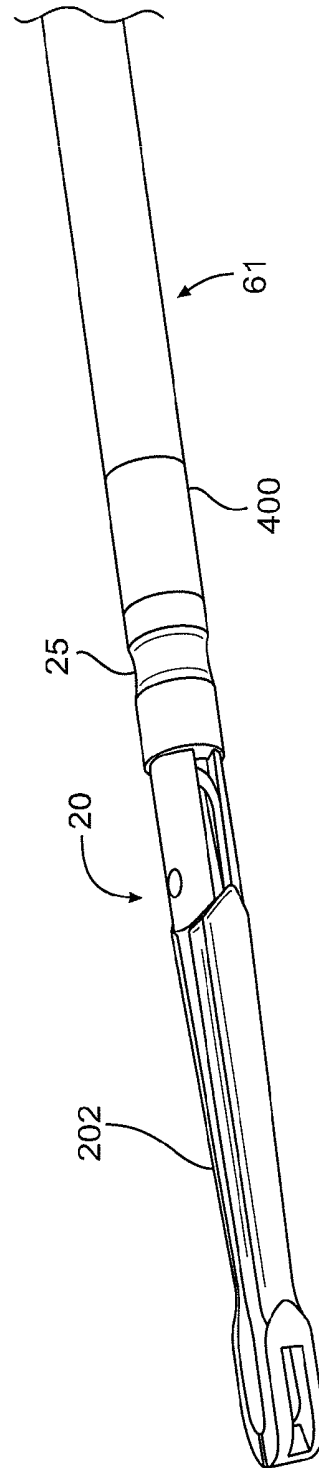


FIG. 2

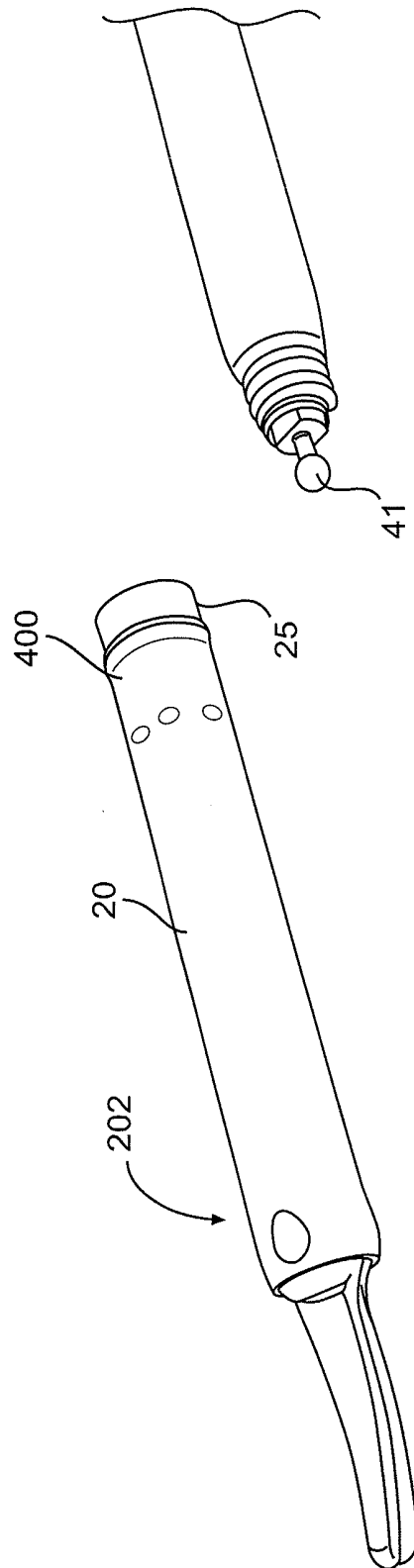


FIG. 3

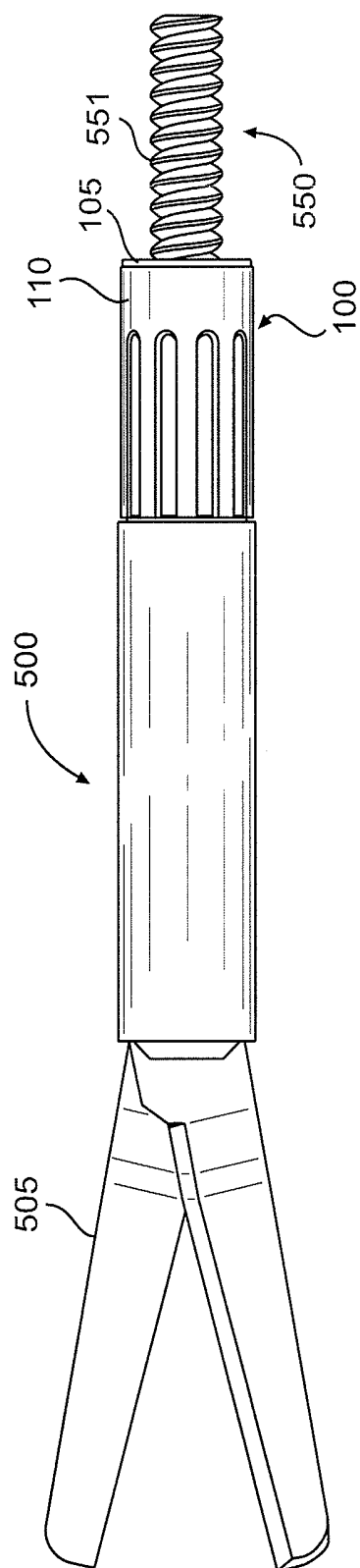


FIG. 4

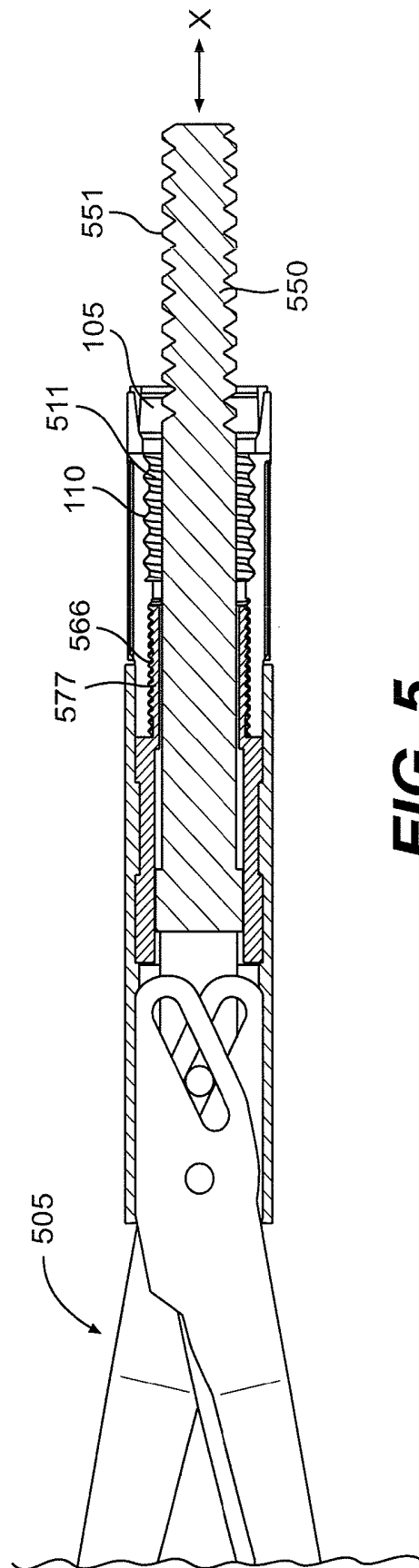
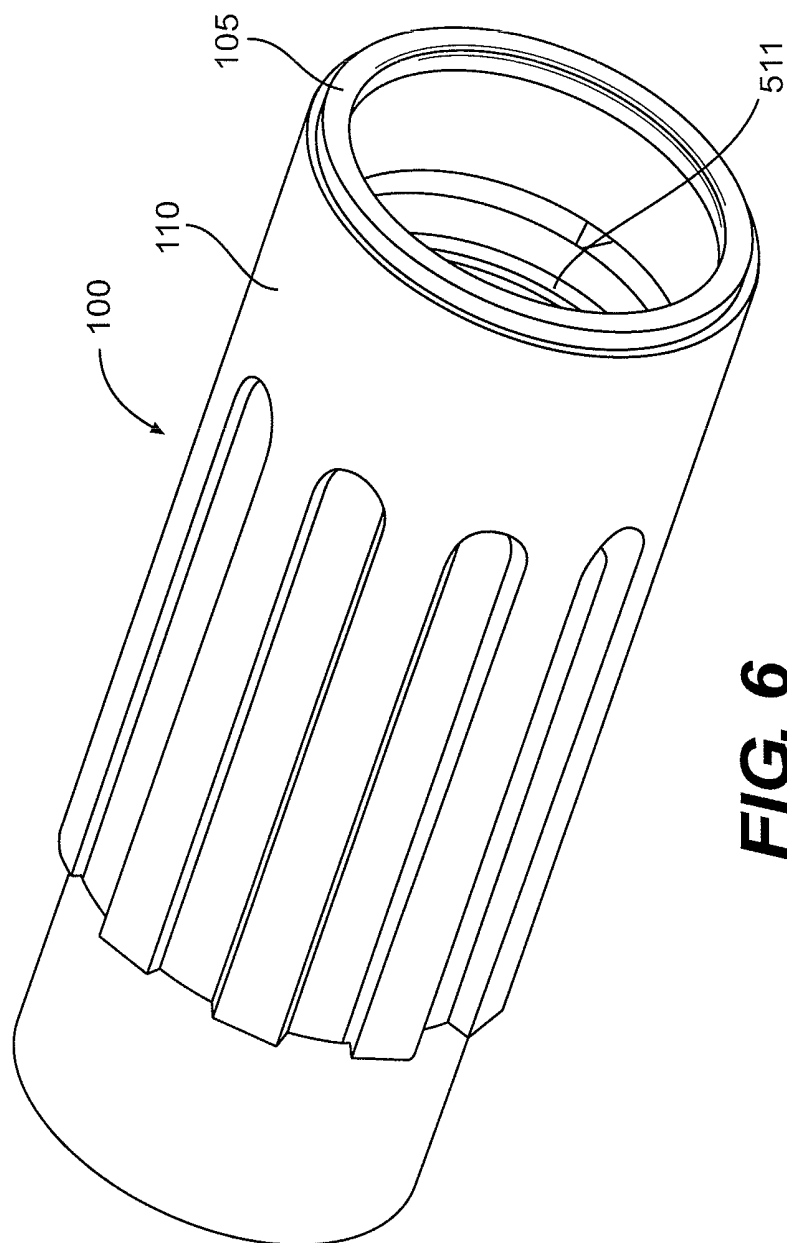


FIG. 5



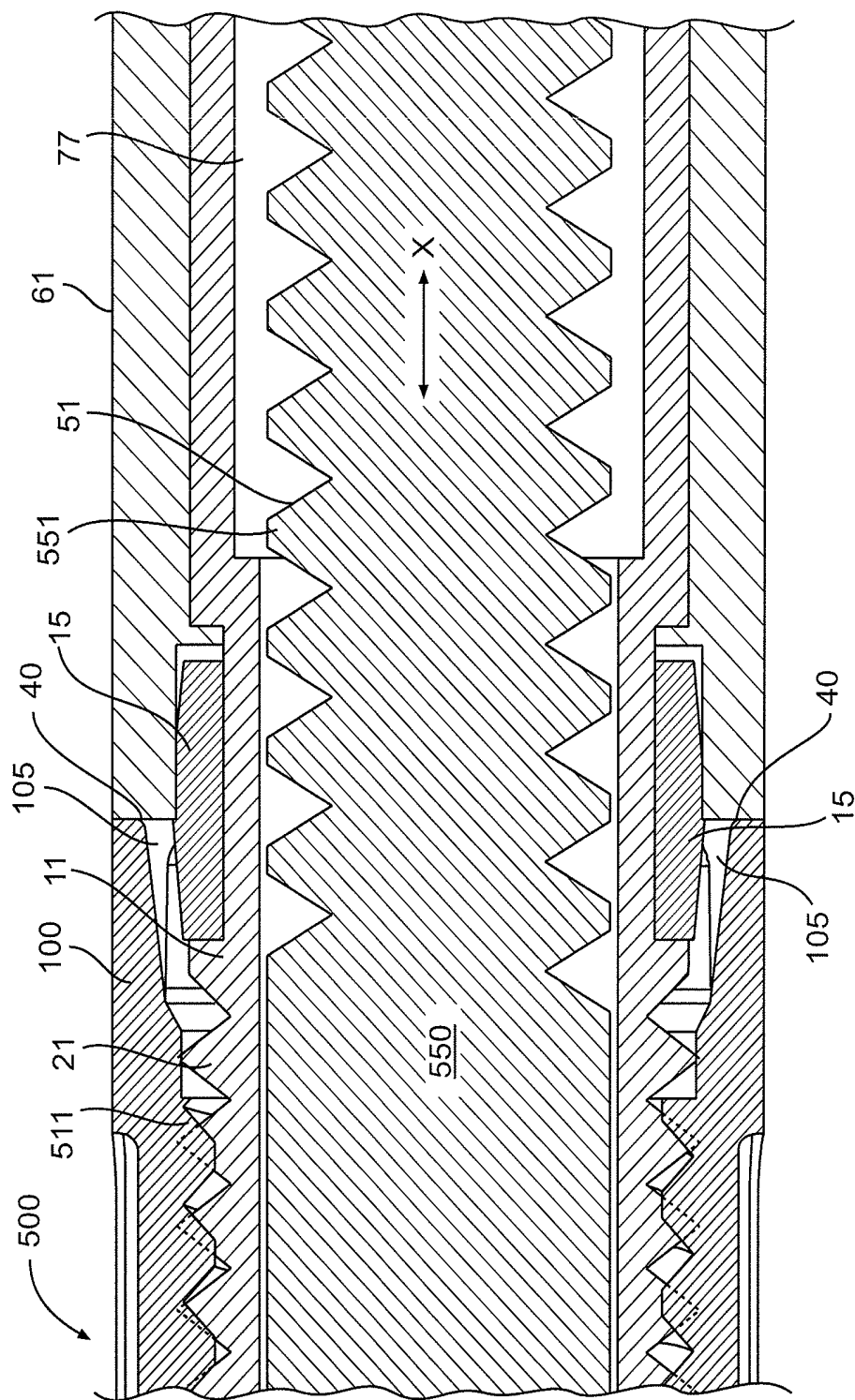


FIG. 7

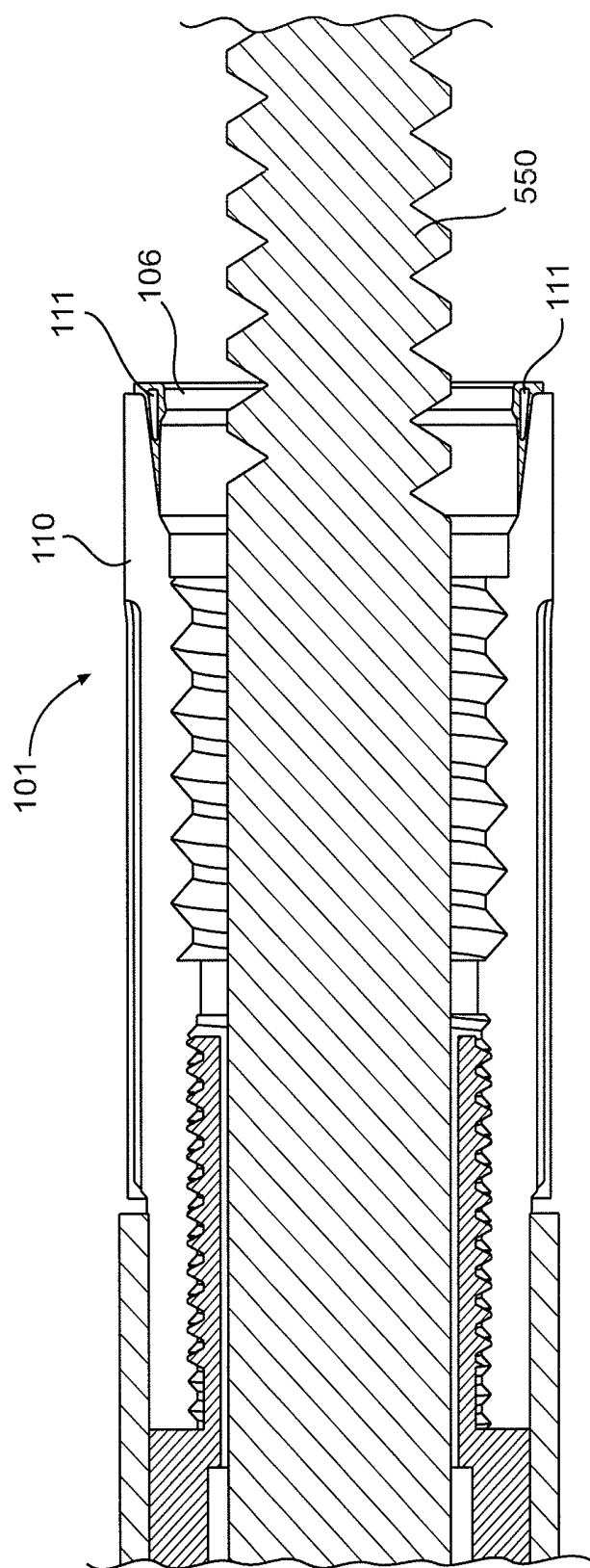


FIG. 8

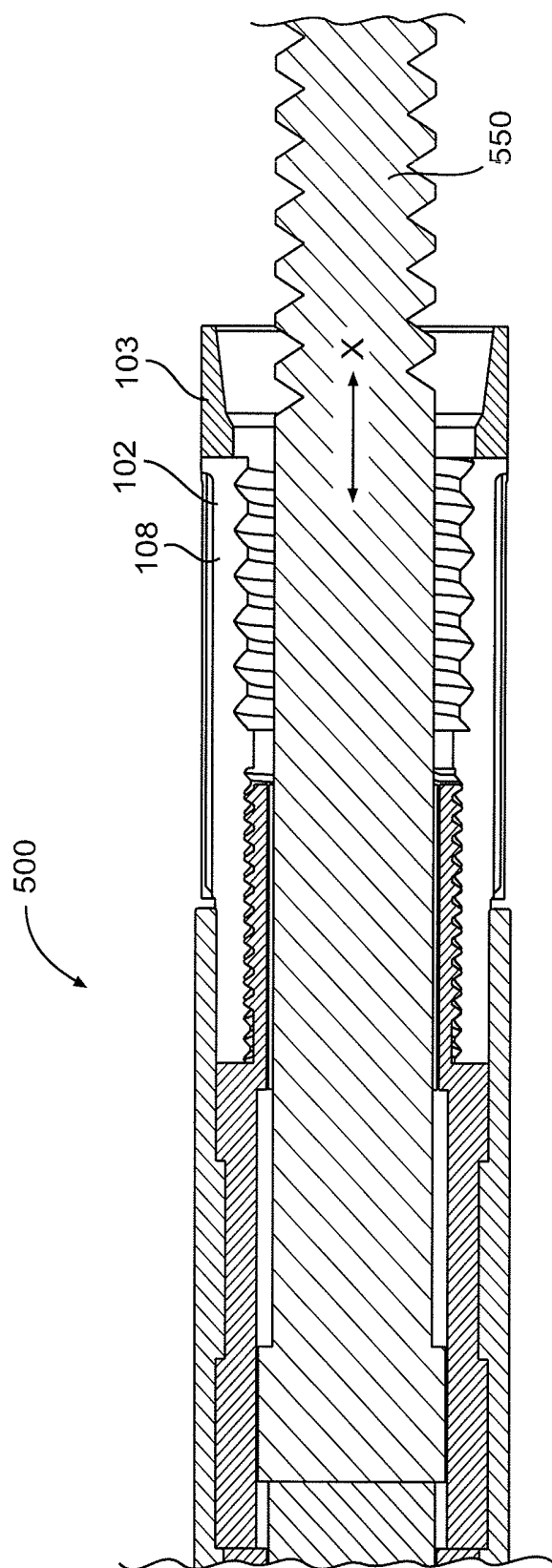


FIG. 9

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CONNECTOR FOR A LAPAROSCOPIC SURGICAL SYSTEM

CLAIM FOR PRIORITY

This application claims the benefit of priority to U.S. Provisional Application No. 61/485,263, filed May 12, 2011, the contents of which are expressly incorporated by reference herein.

BACKGROUND

1. Field of the Invention

This invention relates to an instrument including an electrosurgical apparatus, such as a laparoscopic tube end used for performing laparoscopic, pelvoscopic, arthroscopic, thoroscopic and/or similar such procedures, and more particularly to an electrosurgical apparatus having a connector for fluidically sealing, isolating and electrically insulating a detachable tip when engaged with a laparoscopic tube end.

2. Background of the Invention

Medical procedures such as laparoscopy and the like, which employ a tip at the end of a tube for insertion into the patient, are beneficial because the incisions necessary to perform them are minimal in size, therefore promoting more rapid recovery and lower costs. For example, a patient who undergoes laparoscopic surgery may typically return to normal activity within a period of a few days to about a week, in contrast to more invasive procedures requiring a relatively larger incision (which may require about a month for recovery). Although the term "laparoscopic" is typically used hereinafter, such use of the term "laparoscopic" should be understood to encompass any such similar or related procedures such as, for example, arthroscopic, endoscopic, pelvoscopic and/or thoroscopic or the like, in which relatively small incisions are used.

However, when a tip is detachably connected to the tube end of a laparoscopic device, complications may occur if fluid breaches the connection and enters the interior of the tip or tube end. For example, septic contamination may arise in the laparoscopic device and/or electrical current may unintentionally leak therefrom. After each laparoscopic procedure, the device is also exposed to brushing, chemicals for cleaning and/or sterilization by various methods which may include heating, cooling, and flushing with additional chemicals. The seal in the handpiece may degrade to the point where it loses its integrity (either over use of hundreds of cycles, or from handpiece abuse; which can result in unintended cautery causing damage and injury to structures around a surgical site).

The practice of reprocessing and reusing single-use devices (SUDs) has become increasingly more common because of costs savings and the reduction in waste. However, reprocessed SUDs, such as cutting blades, often do not function as well as SUDs that have not been reprocessed. For example, in the case of reprocessing a cutting blade, the blade may be dulled during the surgical procedure or may be damaged during the reprocessing process such that the cutting blade no longer cuts or opens and closes with the desired or required precision. Further, due to the extensive nooks and crannies, SUD's often cannot be thoroughly sterilized. Therefore, a reprocessed tip, such as those including a cutting blade, may not operate as well after reprocessing any may even result in harm to the patient. Therefore, it is possible that any subpar operation of the reprocessed tip may be incor-

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rectly attributed to the original manufacturer of the reprocessed tip, which may result in damage to the reputation of the original manufacturer.

FIG. 1 shows a tube end **11** of a reusable handpiece **200** to which a conventional tip (which may be a SUD) **20** may be removably attached. The tip has an end effector **202** in the form of a scissors, grasper and the like. The tube end **11** distally extends from a tube **61**, which in turn distally extends from the handpiece having handles (or other suitable controls, not shown, for actuating the tip **20**) operable by the medical personnel or physician performing the surgery. The tube end **11** includes an elastomeric tube end seal **15**, which is typically made from EPDM (ethylene propylene diene monomer). It is often difficult for users to detect when a seal **15** has worn to the point where integrity has been lost. Once integrity is lost, collateral damage can occur any time electrosurgical energy is applied to the device. In the illustrated device, the laparoscopic surgical tip **21** is assembled to the tube of the handpiece **200** using a dual-threaded threaded connector. In other words, the tip **20** includes a yoke **150** having external threading **551**, which engages complementary internal threading on an actuation rod (not shown) extending along the length of the tube **61** (thereby providing for the actuation of the end effector), and a back hub **400** includes internal threading (not shown) which engages complimentary external threading **21** on the tube end **11** to secure the back hub to the tube **61**. Such an attachment typically creates a 50 pound load on the attached components. The seal **15** on the handpiece **200** is compressed by the back hub to create a barrier for electricity and fluids. FIG. 2 shows an surgical tip affixed to a handpiece **200** of FIG. 1 with a heat shrink **25**.

FIG. 3 illustrates a laparoscopic device in which, rather than a seal **15**, a piece of flared heat shrink **25** is used on the disposable tip **20** to create a seal with the tube **61**. Also, the device of FIG. 3 does not use the dual-threaded design of FIGS. 1-2, but instead uses a single threaded connection (between the tube end and the back hub) and a ball **41**-and-clevis arrangement to connect the actuation rod to the yoke (for actuation of the end effector).

SUMMARY OF THE INVENTION

A connector formed from at least two materials for use with a laparoscopic device to interface a tube end with a tip end. The connector includes a rigid base and a seal that are integrally formed to provide a connection between the tube end and the tip end that is electrically insulative and protects against fluid intrusion.

In one embodiment, there is a connector in the form of a laparoscopic instrument tip for interfacing with a laparoscopic tube end, the laparoscopic instrument tip including a base forming a body of the connector, the base being electrically insulative and configured to interface with the tube end and the instrument tip, and a seal integrally formed with the base, the seal having an engagement part on at least one side and expanding upon being engaged.

In one aspect, the engagement part engages with at least one of the tube end and the instrument tip, thereby fluidically sealing and electrically insulating the connection therebetween.

In yet another aspect, the base is rigid and formed as one of a cylindrical shape, circular shape, square shape, rectangular shape and triangular shape.

In another aspect, the integrally formed base and seal are formed as a single component and from different materials. In still another aspect, the seal includes a plastic material encas-

ing a fluid, whereby the fluid is released and acts as an insulative material upon being engaged.

In another aspect, the seal is at least partially destroyed upon being engaged with at least one of the tube end and the instrument tip.

An aspect provides a connector for connecting an instrument tip with a laparoscopic tube end, the connector having a base forming a body of the connector, the base having a lumen configured to accommodate an instrument tip actuator therein, and a seal permanently bonded to an inner surface of a proximal end of the base and configured to deform upon connection of the connector with the tube end.

In a further aspect, when the connector connects to the tube end, the instrument tip actuator is electrically insulated and fluidically sealed from the outside of the tube end. Further, the connector may be unitarily formed with the instrument tip.

In another aspect, the connector can further include an engagement region on at least one of the base and the seal, wherein the engagement region is one of threaded, press-fit, bayonet, ball-and-detent, barrel pin, dog-tooth ratchet mechanism, and the engagement region is configured to engage a complimentary engagement region on the tube end. Further, in a non-limiting aspect, when the connector connects to the tube end, the seal is not visible from the exterior of the connector and tube end.

In yet another aspect, the seal may be chemically bonded to the base by a chemical bonding agent. Also, the base material may be more rigid than the seal material.

In a further aspect, the seal is permanently deformed upon being engaged with the tube end. Also, at least one of the base and seal is one of permanently, dissolved, deformed and destroyed after a predetermined number of uses or predetermined amount of time.

In another aspect, the base includes at least one of a recess and protrusion on the inner surface thereof, and the seal is permanently mechanically bonded to the at least one of the recess and protrusion.

In yet another aspect, a distal end of the base is configured to removably attach to a proximal end of the instrument tip. Also, the distal end of the base may be configured to removably threadably attach to the proximal end of the instrument tip.

In still another aspect, the seal proximally extends from the base when the connector is unattached to the tube end, and the base fits flush against the tube end when the connector is attached to the tube end. In a further aspect, an outer diameter of the seal extends radially outwardly beyond an inner diameter of the base when the connector is unattached to the tube end, and the outer diameter of the seal is within the inner diameter of the base when the connector is attached to the tube end.

Also, an outer diameter of the seal may be less than an outer diameter of the base.

In a further aspect, at least one of the base and seal at least one of deforms, degrades and dissolves when exposed to chemical or heat sterilization.

In another aspect, provided is a laparoscopic device, including a tube end having an outer tube end and an inner shaft, an instrument tip configured to engage with the tube end, and a connector having a base and seal, the seal having an engagement part on at least one side and expanding upon being engaged with at least one of the tube end and the tip end.

In a further aspect, provided is a laparoscopic device, having a tube having a lumen and a slidable inner shaft, an instrument tip configured to be affixed to a distal end of the tube, and a connector affixed to a proximal end of the instru-

ment tip having a back hub and seal permanently bonded to the back hub, the seal configured to deform upon engaging the tube.

In an additional aspect, the instrument tip and the connector are unitarily formed together. Also, the tube may electrically insulate and fluidically seals the inner shaft from the outside of the tube end.

In another aspect, the back hub is one of threaded, press-fit, bayonet, ball-and-detent, barrel pin, dog-tooth ratchet mechanism. Also, the seal may include at least one fluid-encased pocket, wherein upon deformation of the at least a portion of the seal, the pocket is ruptured and fluid is released. Further, the seal may be at least partially visible when the connector is connected to the tube.

In yet another aspect, at least one of the back hub and seal is one of permanently deformed, dissolved and destroyed after a predetermined number of uses or predetermined amount of time.

In another aspect, the base is rigid and formed as one of a cylindrical shape, circular shape, square shape, rectangular shape and triangular shape.

In still another aspect, the integrally formed base and seal are formed as a single component and from different materials.

In another aspect, the seal includes a plastic material encasing a fluid, whereby the fluid is released and acts as an insulative material upon being engaged. The seal may include at least one fluid-encased pocket, wherein upon deformation of the at least a portion of the seal, the pocket is ruptured and fluid is released.

In still another aspect, the seal is at least partially visible when the connector is interfaced with at least one of the tube end and instrument tip.

In another aspect, the seal is at least partially destroyed upon being engaged with at least one of the tube end and the instrument tip.

According to a further aspect, provided is a connector for connecting an instrument tip with a laparoscopic tube end, the connector having a base forming a body of the connector, the base having a lumen configured to accommodate an instrument tip actuator therein, and a seal configured to deform upon connection of the connector with the tube end, wherein the base and seal are formed of a single unitary material, and wherein one of the base and seal are subject to one of chemical, optical and radiological exposure, such that the seal is more flexible than the base.

Another feature of the invention provides an instrument tip configured to be connected to a tube end, the instrument tip having a back hub having a hollow center configured to accommodate an end effector actuator therein, an end effector configured to engage a target, wherein the end effector actuator configured to actuate the end effector, and an elastomeric seal permanently bonded to an inner surface of the back hub and configured to deform upon connection of the connector with the tube end.

According to another aspect, the end effector actuator is a yoke configured to mechanically actuate the end effector, and a proximal end of the yoke is configured to attach to an axially slidable rod located in the tube end.

According to another aspect, the back hub comprises threading on an inside surface thereof, the threading configured to engage complimentary threading on the tube end, the end effector actuator is a yoke configured to mechanically actuate the end effector, and a proximal end of the yoke includes yoke threading configured to threadably attach to complimentary threading on an axially slidable rod located in the tube end.

According to a further aspect, the back hub includes at least one of a recess and protrusion on the inner surface thereof, and the seal is permanently mechanically bonded to the at least one of the recess and protrusion. Additionally, the seal may be chemically bonded to the base by a chemical bonding agent.

Also provided is a method of forming a connector configured to attach to a tube end, the method including molding a connector base having a hollow center and at least one of a recess and protrusion on the inner surface of the connector base, placing the connector base inside a mold, extruding liquid silicon material into the mold such that the liquid silicon material permanently mechanically bonds to the at least one of a recess and protrusion, to form a seal on a proximal end of the connector base, upon curing of the silicon material.

Further provided is a method of forming a connector configured to attach to a tube end, the method including, molding a connector base having a hollow center, placing the connector base inside a mold, and extruding liquid silicon material and a bonding agent into the mold such that the liquid silicon material permanently chemically bonds to an inner surface of the connector base to form a seal on a proximal end of the connector base, upon curing of the silicon material.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 shows a perspective view of an end of a reusable handpiece with a conventional seal;

FIG. 2 shows a perspective view of an assembled embodiment of a laparoscopic surgical tip of FIG. 1;

FIG. 3 shows a perspective view of a prior art laparoscopic device in which a piece of flared heart shrink is used on a disposable tip to create a seal to the handpiece;

FIG. 4 shows a side elevational view of an exemplary embodiment of a connector for an instrument tip in accordance with a non-limiting aspect of the disclosure;

FIG. 5 shows a side sectional view of the connector and instrument tip of FIG. 4;

FIG. 6 shows a perspective view of the connector in accordance with a non-limiting aspect of the disclosure;

FIG. 7 shows a side sectional view of the connector in accordance with a non-limiting aspect of the disclosure connected to a laparoscopic tube end;

FIG. 8 shows a side sectional view of the connector in accordance with a second non-limiting embodiment; and

FIG. 9 shows a side sectional view of the connector in accordance with a third non-limiting embodiment.

DETAILED DESCRIPTION

The particulars shown herein are by way of example and for purposes of illustrative discussion of the embodiments of the present invention only, and are presented for providing what is believed to be the most useful and readily understood description of the principles and conceptual aspects of the present invention. In this regard, no attempt is made to show structural details of the present invention in more detail than is necessary for the fundamental understanding of the present invention, the description taken with the drawings making apparent to those skilled in the art how the several forms of the present invention may be embodied in practice.

FIGS. 4-7 show an exemplary embodiment of a connector of a laparoscopic instrument tip in accordance with a non-limiting aspect of the disclosure. A laparoscopic instrument tip 500 is attachable to a reusable handpiece 200 (described in relation to FIGS. 1-2) and is used for performing a minimally-

invasive laparoscopic procedure such as excision of tissue with cauterization. The tip 500 may typically include (but is not limited to) a tip 500 having an end effector 505 (which may or may not be electrified) such as a grasper, ligation tool, blade, shears, a cauterization tool and the like, in which the tip 500 may engage with the tube end 11 of a tube 61 which extends from a base portion connected to handles (or other suitable control device, not shown) operable by the medical personnel or physician performing the surgery.

As best shown in FIG. 7, the tip 500 includes a tip actuator in the form of, e.g., a yoke 550 having external threading 551, which engages complementary internal threading 51 on an actuation rod 77 extending along the length of the tube 61 and slidable in direction X relative to the tube (thereby providing for the actuation of the end effector), and the connector 100 includes internal threading 511 which engages the complimentary external threading 21 on the tube end 11 to secure the connector 100 to the tube 61. In this embodiment, the connector 100 serves as a back hub and may also be termed as such herein. Although the figures show the connector 100 connecting the tip to the tube 61 using the above-described a dual-threaded attachment mechanism, those skilled in the art will appreciate that a single-threaded (or no-threaded) attachment mechanism may be employed. In a single-threaded attachment arrangement, while the connector 100 includes internal threading 511 which engages the complimentary external threading 21 on the tube end 11, the yoke 550 and actuation rod 77 can connect by other mechanisms, including but not limited to press-fit, bayonet, ball-and-detent, barrel pin, dog-tooth ratchet mechanism and the like. In a no-threaded attachment mechanism, the connector 100 may not employ a threaded design. As an alternative to internal threading 511 which engages the complimentary external threading 21 on the tube end 11, the connector may employ any form of any suitable engagement technology including but not limited to press-fit, bayonet, ball-and-detent, barrel pin, dog-tooth ratchet mechanism and the like. It is also noted that while the tip actuator is shown as a yoke 550 configured to move in the X direction relative to the tube 61, those skilled in the art will appreciate that the tip actuator need not move (e.g., in the event that the end effector is stationary).

The connector 100 includes seal 105 (discussed below) and according to a non-limiting aspect, is threadably affixed to the tip 500. For example and as shown in FIG. 5, the distal end of the connector 100 may include internal threading 566 to threadably engage external threading 577 on the proximal end of the tip 500, although those skilled in the art will appreciate that the connector may have the external threading and the tip may have the internal threading. Although the figures show the connector 100 threadably attached to the tip 500, those skilled in the art will also appreciate that the connector and tip may be connected by other means (including but not limited to press-fit, bayonet, ball-and-detent, barrel pin, dog-tooth ratchet mechanism and the like), and that the connector and cylindrical tip portion may be unitarily formed from a single piece of material.

FIG. 6 shows an exemplary embodiment of the connector 100. The connector 100, as illustrated, shows an elastomeric seal 105 provided in a cylindrically-shaped base 110 (i.e., the portion of the connector other than the seal) made of a material that is more rigid than the material of which the seal is formed. According to a feature of the disclosure, when using mechanical bonding (mechanical interlocking) between the seal 105 and the base 110, the base is formed from polyphenylsulfone (PPSU) (commonly referred to by the trade name Radel®), or may be formed from Polysulphone (PSU) (commonly referred to by the trade name Udel®), although those

skilled in the art would appreciate that any suitable mid-range or higher polymer may be used.

According to a feature of the disclosure, the seal **105** is formed from a flexible material such as silicone, although those skilled in the art would appreciate that any suitable flexible material may be used. For a chemically-bonded connection between the seal **105** and the base **110**, the exact material of the base **110** and of the seal **105** may be selected based on the type adhesive in the silicone. It is noted that the base **110** or seal **105** may be constructed of material that deforms, degrades or dissolves when exposed to chemical or heat (e.g., autoclaving) sterilization. In this way, the tip **500** is prevented from being reused.

The seal **105** may be unitarily formed (from a single piece of material) with the base **110** or may be formed separate from the base **110**, as explained below. Likewise, base **110** need not be made of a rigid material, but may provide for an acceptable degree of flexibility, so long as the base is more rigid than the seal **105**. In this regard, the connector **100** includes at least two materials which together form a single component. This integration allows the selection of materials for the base **110** and seal **105** to have mutually exclusive requirements. In a non-limiting aspect, the connector **100** is formed to be strong, rigid and electrically insulative, while at the same time creating a compliant connection (in the form of the seal **105**) that protects against fluid intrusion. It is appreciated that the connector **100** may be formed in any suitable shape, and is not limited to the specific shape disclosed in the drawings.

Although the figures show the length of seal **105** only partially extending inside the base **110** in the X direction, it is appreciated by those skilled in the art that the seal may be of any suitable length in the X direction (including extending the entire length of the base **110**). In this regard, while the figures show the internal threading **511** is being formed of the same rigid material as the base, it is appreciated by those skilled in the art that the seal **105** may also include the internal threading.

The seal **105** of the connector **100** either supports (supplements) or replaces, for example, the function of the tube end seal **15** on the reusable handpiece illustrated in FIG. **1**. The connector **100** may be rigid and electrically insulative, or may be either entirely or partially formed of an elastomeric material including, but not limited to, for example, natural or artificial rubber, plastic (such as, for example, polyethylene, polypropylene, PPSU, PSU or any other suitable plastic polymer), and/or resin (and/or any suitable mixture or compound thereof, noting that the elastomeric material is not limited to the exemplary materials thus noted). Further, the seal **105** may be formed from a different material than the base **110**, at one or both ends that may be unitarily integrated into the base **110** to form the connector **100**. The seal **105** may also be formed such that it is not unitarily formed with the base **110**, but rather formed separately and bonded to the base **110**.

As shown in FIG. **4**, in the unattached state, the seal **105** proximally extends past the base **110** in the X direction, and (as shown in FIGS. **4-5**) the outer diameter of the seal further extends radially outwardly beyond the inner diameter of the base. As shown in FIG. **7**, the connector **100** is threadably attached to the tube end **11**, the seal **105** deforms against the distalmost portion of the tube **61** (flange **40**) and if forced radially inwardly toward the outside of the tube end seal **15**, such that the seal **105** no longer proximally extends past the base **110** in the X direction or extends radially outwardly beyond the inner diameter of the base, so that the outer diameter of the assembled device is not interrupted by the seal. As such and as shown in FIG. **7**, when attached, the connector abuts flush directly against the distalmost portion of the tube

61 at the tube end **11**. In the event that during attachment of the tip **500** to the tube **61** end and the seal **105** is visible to the user, the user may note that there is an error in attaching the tip **500** to the tube **61**, and that the tip should be reattached or a different tip should be used. To this effect, the seal **105** may be of a color contrasting with the colors of the connector **100** and tube **61**. It is preferred that the connector **100**, tip **500** and tube **61** have the same outer diameter for ease of operation.

The ability of the connector **100** to conform to the handpiece **200** offers additional sealing redundancy at the junction when used in conjunction with other sealing members, such as the tube end seal **15** (although it is noted that the seal **105** may replace the tube end seal). This redundancy allows a handpiece **200** to be used safely, regardless of the tube end seal **15** condition. It is appreciated that the connector **100** may be formed in any desired shape, and is not limited to the specific embodiments disclosed in the drawings.

This attachment of the tip **500** to the tube **61** as shown in FIG. **7** seals the interior of the laparoscopic tube end **11** (i.e., the cavity where the yoke **550** and rod **77** operate) from any fluids surrounding the tip **500** or tube end **11**, and electrically insulates and fluidically isolates the laparoscopic tube end **11** from the exterior of the tube **61** and tip **500** because the pressure between the distalmost portion of the tube **61** (flange **40**) and seal **105** and the adhesiveness and elasticity of the seal **105** form a fluidic seal, and the electrically insulating properties of the elastomeric material of the seal **105** form a high electrical impedance. In addition, the pressure of the seal **105** in the connector **100**, when fully engaged against the flange **40**, may beneficially prevent rotation and/or disengagement of the connector **100** from the laparoscopic tube end **11**, because the frictional resistance resulting from the abutment of the seal **105** of the connector **100** against the flange **40** tends to prevent rotation and unscrewing of the connector **100** from the tube end **11**. The composition, shape and/or materials of the seal **105** and/or connector **100** may be selected to optimize the frictional contact with the seal **105**, the effectiveness of the fluidic seal, and/or the effectiveness of the electrical impedance thereof, for example.

In accordance with a non-limiting feature, the connector **100** is formed using an insert molding process. In such a process, the formed base **110** is inserted into a mold, whereupon the seal material (e.g., silicone) is extruded into the mold and bonded to the base to create the connector. The seal **105** may be chemically and/or mechanically bonded to the base **110**. In the case of chemical bonding, the seal material, combined with a chemical bonding agent (e.g., an adhesion promoter), is extruded into the mold, whereupon during the curing process, the seal **105** permanently and chemically bonds to the base **110** and cannot be removed from the base without destroying the connector **100**.

In the case of mechanical bonding, the portion of inside of the base **110** to interface with the seal **105** includes one or more recesses (e.g., a recessed channel), one or more protrusions or a combination thereof for accepting the seal material therein. The seal material (without a chemical bonding agent) is then extruded into the mold and extrudes into the recess(es) and/or over protrusion(s) and then cures. The action of molding the seal **105** in place creates a mechanically-integrated, permanently-bonded component (connector **100**) which has two sets of material properties. The recess/protrusion combination increases the surface area of the inside of the base **110** for contacting the seal **105**, and as such, removal of the seal from the base cannot be done without destroying the connector **100**. It will also be appreciated that a combination of chemical and mechanical bonding between the seal **105** and base **110** can be performed.

In accordance with another non-limiting feature, the connector **100** is formed using an double molding process. In this process, a primary molding material (base **110**) is first poured in a mold. After the primary molding (base **110**) is formed, a secondary molding material (seal **105**) poured is added to the same mold to form a composite, double-molded connector. It is noted that the above-described chemical and/or mechanical bonding process may be used in the double-molding process.

In accordance with a further non-limiting embodiment, the seal **105** includes a flexible material (such as a flexible ring) that may separately formed from the base **110** (e.g., by molding) and then inserted or placed into the base **110** to form the connector **100**. In this embodiment, the connector **100** is formed of the base **110** and seal **105**, without the seal having to be bonded or unitarily formed with the base into the connector **100**.

FIG. **8** shows another embodiment of a connector **101**, in which a seal **106** includes one or more pockets **111** encasing a viscous fluid. Once compressed, pressure from the compression results in the pocket(s) being breached or ruptured, releasing a fluid (including but not limited to a silicone fluid) inside the connector **101**. In other words, upon assembly of the connector **101** with the tube **61**, the fluid is compressed out of the pocket(s) **111** to flood any clearances left in the connector-tube junction. The released fluid may act as an additional insulation material. Further, since the breached pockets alter the dimensions of the seal, re-use of the tip **500** is further prevented.

In additional embodiments, the seal **105** can be fully or partially visible to the user (and may be of contrasting color to the base **110** and tube **61**), thereby providing visual confirmation of the tip's **500** proper installation. The seal **105** may also be designed for a single application to the tube end **11** such that the seal **105** can get partially or fully dissolved, deformed or destroyed upon use (or multiple uses, fixed or otherwise), thereby preventing the tip **500** from being reused. In other words, the inner material of the seal **105** may be configured such that once the outer surface of the tube end **11** (e.g., threading **21**) engages the inner material of the seal (e.g., complementary threading **511**) to attach the tip **500** to the tube **61**, the inner material is permanently deformed such that upon disengagement of the tube end and the tip, the tube end and the tip cannot be securely (i.e., successfully enough for the instrument **65** to be used in a medical procedure) reattached. In this way, the tip **500** is prevented from being reused.

FIG. **9** shows a connector **102** according to a further embodiment. Rather than providing a connector **100** including at least two materials bonded to form a single component as described above a connector **102** is formed of a single unitary type of material, a portion of which is treated to alter the material properties thereof, such that the connector has two different elastomeric properties at respectively two different regions in the X direction. In other words, a portion of the connector **102** is treated chemically (via application of a chemical), optically (via application of light) or radiologically (via application of radiation) to render the portion harder or softer than the remainder (untreated portion) of the connector **102**. As an example, if the connector **102** is formed of PTFE (Polytetrafluoroethylene), and a portion **108** is irradiated, this portion **108** will become hard (harder than the non-irradiated portion **103**, which can then serve as the seal). It is noted that such treatment of the connector can be performed before or after the tip **500** is attached to the tube **61**.

In view of the foregoing, the present disclosure, through one or more of its various aspects, embodiments and/or specific features or sub-components, is thus intended to bring out

one or more of the advantages as specifically noted below. While the present disclosure includes description with respect to a medical device and procedure, the present invention may be used in a variety of other, non-medical, environments.

The illustrations of the embodiments described herein are intended to provide a general understanding of the structure of the various embodiments. The illustrations are not intended to serve as a complete description of all of the elements and features of apparatus and systems that utilize the structures or methods described herein. Many other embodiments may be apparent to those of skill in the art upon reviewing the disclosure. Other embodiments may be utilized and derived from the disclosure, such that structural and logical substitutions and changes may be made without departing from the scope of the disclosure. Additionally, the illustrations are merely representational and may not be drawn to scale. Certain proportions within the illustrations may be exaggerated, while other proportions may be minimized. Accordingly, the disclosure and the figures are to be regarded as illustrative rather than restrictive.

One or more embodiments of the disclosure may be referred to herein, individually and/or collectively, by the term "invention" merely for convenience and without intending to voluntarily limit the scope of this application to any particular invention or inventive concept. Moreover, although specific embodiments have been illustrated and described herein, it should be appreciated that any subsequent arrangement designed to achieve the same or similar purpose may be substituted for the specific embodiments shown. This disclosure is intended to cover any and all subsequent adaptations or variations of various embodiments. Combinations of the above embodiments, and other embodiments not specifically described herein, will be apparent to those of skill in the art upon reviewing the description.

The Abstract of the Disclosure is submitted with the understanding that it will not be used to interpret or limit the scope or meaning of the claims. In addition, in the foregoing Detailed Description, various features may be grouped together or described in a single embodiment for the purpose of streamlining the disclosure. This disclosure is not to be interpreted as reflecting an intention that the claimed embodiments require more features than are expressly recited in each claim. Rather, as the following claims reflect, inventive subject matter may be directed to less than all of the features of any of the disclosed embodiments. Thus, the following claims are incorporated into the Detailed Description, with each claim standing on its own as defining separately claimed subject matter.

The above disclosed subject matter is to be considered illustrative, and not restrictive, and the appended claims are intended to cover all such modifications, enhancements, and other embodiments which fall within the true spirit and scope of the present disclosure. Thus, to the maximum extent allowed by law, the scope of the present disclosure is to be determined by the broadest permissible interpretation of the following claims and their equivalents, and shall not be restricted or limited by the foregoing detailed description.

What is claimed is:

1. A connector for connecting an instrument tip with a laparoscopic tube end, the connector comprising:

a base forming a body of the connector, the base having a lumen configured to accommodate an instrument tip actuator therein; and

a seal permanently and chemically bond molded to an inner surface of a proximal most end of the base and configured to deform upon connection of the connector with

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the tube end such that upon disengagement of the connector and the tube end, the seal is deformed such that the tube end and the tip cannot be securely reattached.

2. The connector of claim 1, wherein when the connector connects to the tube end, the instrument tip actuator is electrically insulated and fluidically sealed from the outside of the tube end.

3. The connector of claim 1, further comprising an engagement region on at least one of the base and the seal, wherein: the engagement region is one of threaded, press-fit, bayonet, ball-and-detent, barrel pin, dog-tooth ratchet mechanism, and the engagement region is configured to engage a complementary engagement region on the tube end.

4. The connector of claim 1, wherein when the connector connects to the tube end, the seal is not visible from the exterior of the connector and tube end.

5. The connector of claim 1, wherein the seal comprises at least one fluid-encased pocket, wherein upon deformation of at least a portion of the seal, the pocket is ruptured and fluid is released.

6. The connector of claim 1, wherein the seal is permanently deformed upon being engaged with the tube end.

7. The connector of claim 1, wherein at least one of the base and seal is one of permanently dissolved, deformed and destroyed after a predetermined number of uses or predetermined amount of time.

8. The connector of claim 1, wherein the base material is more rigid than the seal material.

9. The connector of claim 1, wherein a distal end of the base is configured to removably attach to a proximal end of the instrument tip.

10. The connector of claim 9, wherein the distal end of the base is configured to removably threadably attach to the proximal end of the instrument tip.

11. The connector of claim 1, wherein:
the seal proximally extends from the base when the connector is unattached to the tube end; and
the base fits flush against the tube end when the connector is attached to the tube end.

12. The connector of claim 1, wherein an outer diameter of the seal is less than an outer diameter of the base.

13. The connector of claim 1, wherein at least one of the base and seal at least one of deforms, degrades and dissolves when exposed to chemical or heat sterilization.

14. The connector of claim 1, wherein:
an outer diameter of the seal extends radially outwardly beyond an inner diameter of the base when the connector is unattached to the tube end; and
the outer diameter of the seal is entirely within the inner diameter of the base when the connector is attached to the tube end.

15. The connector of claim 1, wherein:
the base comprises internal threading; and
the seal is permanently bonded to the inner surface of the base at a position proximal to the internal threading.

16. The connector of claim 1, wherein the seal proximally protrudes from the proximal most end of the base.

17. The connector of claim 1, wherein the seal is of a color contrasting with a color of the base.

18. The connector of claim 1, wherein the seal is permanently, adhesively and chemically bond molded to the inner surface of the proximal most end of the base.

19. A connector for connecting an instrument tip with a laparoscopic tube end, the connector comprising:
a base forming a body of the connector, the base having a lumen configured to accommodate an instrument tip

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actuator therein, the base comprising at least one of a recess and protrusion on the inner surface of a proximal most end of the base; and

a seal permanently mechanically bond molded to the at least one of the recess and protrusion, wherein the seal is configured to deform upon connection of the connector with the tube end, such that upon disengagement of the connector and the tube end, the seal is deformed such that the tube end and the tip cannot be securely reattached.

20. A laparoscopic device, comprising:
a tube having a lumen and a slidable inner shaft;
an instrument tip configured to be affixed to a distal end of the tube; and

a connector affixed to a proximal end of the instrument tip having a back hub and seal permanently bonded to the back hub, the seal configured to deform upon engaging the tube such that upon disengagement of the connector and the tube, the seal is deformed such that the tube and the tip cannot be securely reattached.

21. The laparoscopic device of claim 20, wherein the instrument tip and the connector are unitarily formed together.

22. The laparoscopic device of claim 21, wherein the tube electrically insulates and fluidically seals the inner shaft from the outside of the tube end.

23. The laparoscopic device of claim 20, wherein the back hub is one of threaded, press-fit, bayonet, ball-and-detent, barrel pin, dog-tooth ratchet mechanism.

24. The laparoscopic device of claim 20, wherein the seal includes at least one fluid-encased pocket, wherein upon deformation of the at least a portion of the seal, the pocket is ruptured and fluid is released.

25. The laparoscopic device of claim 20, wherein the seal is at least partially visible when the connector is connected to the tube.

26. The laparoscopic device of claim 20, wherein at least one of the back hub and seal is one of permanently deformed, dissolved and destroyed after a predetermined number of uses or predetermined amount of time.

27. The laparoscopic device of claim 20, wherein the back hub material is more rigid than the seal material.

28. A connector for connecting an instrument tip with a laparoscopic tube end, the connector comprising:

a base forming a body of the connector, the base having a lumen configured to accommodate an instrument tip actuator therein; and

a seal configured to deform upon connection of the connector with the tube end such that upon disengagement of the connector and the tube end, the seal is deformed such that the tube end and the tip cannot be securely reattached,

wherein: the base and seal are formed of a single material, and the seal is more flexible than the base.

29. An instrument tip configured to be connected to a tube end, the instrument tip comprising:

a back hub having a hollow center configured to accommodate an end effector actuator therein;

an end effector configured to engage a target, wherein the end effector actuator configured to actuate the end effector; and

an elastomeric seal permanently bonded to an inner surface of the back hub and configured to deform upon connection of the connector with the tube end such that upon disengagement of the connector and the tube end, the seal is deformed such that the tube end and the tip cannot be securely reattached.

30. The instrument tip of claim 29, wherein:

the end effector actuator is a yoke configured to mechanically actuate the end effector, and

a proximal end of the yoke is configured to attach to an axially slidable rod located in the tube end. 5

31. The instrument tip of claim 29, wherein:

the back hub comprises threading on an inside surface thereof, the threading configured to engage complimentary threading on the tube end;

the end effector actuator is a yoke configured to mechanically actuate the end effector, and 10

a proximal end of the yoke comprises yoke threading configured to threadably attach to complimentary threading on an axially slidable rod located in the tube end.

32. The instrument tip of claim 29, wherein: 15

the back hub comprises at least one of a recess and protrusion on the inner surface thereof; and

the seal is permanently mechanically bonded to the at least one of the recess and protrusion.

33. The instrument tip of claim 29, wherein the seal is 20
chemically bonded to the base by a chemical bonding agent.

* * * * *

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摘要(译)

一种用于连接器械尖端和腹腔镜管端部的连接器，该连接器包括形成连接器主体的基部，基部具有构造成在其中容纳器械尖端驱动器的内腔，以及永久地结合到内表面的密封件。基座的近端并且构造成在连接器与管端部连接时变形。

