

(19)



(11)

EP 1 767 156 B2

(12)

NEW EUROPEAN PATENT SPECIFICATION

After opposition procedure

(45) Date of publication and mention
of the opposition decision:
21.06.2017 Bulletin 2017/25

(51) Int Cl.:
A61B 17/072 ^(2006.01) **A61B 17/00** ^(2006.01)

(45) Mention of the grant of the patent:
26.08.2009 Bulletin 2009/35

(21) Application number: **06254867.2**

(22) Date of filing: **20.09.2006**

(54) **Surgical stapling instrument having force controlled spacing end effector**

Chirurgisches Klammerinstrument mit einem kraftgeregelten Abstand des Endeffektors

Agrafeuse chirurgicale avec un effecteur terminal à espacement contrôlé par la force appliquée

(84) Designated Contracting States:
**AT BE BG CH CY CZ DE DK EE ES FI FR GB GR
HU IE IS IT LI LT LU LV MC NL PL PT RO SE SI
SK TR**

(30) Priority: **21.09.2005 US 231456**

(43) Date of publication of application:
28.03.2007 Bulletin 2007/13

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Description

FIELD OF THE INVENTION

[0001] The present invention relates in general to surgical stapler instruments that are capable of applying lines of staples to tissue while cutting the tissue between those staple lines and, more particularly, to improvements relating to stapler instruments and improvements in processes for forming various components of such stapler instruments including adding bolstering material to the severed and stapled tissue.

BACKGROUND OF THE INVENTION

[0002] Endoscopic and laparoscopic surgical instruments are often preferred over traditional open surgical devices since a smaller incision tends to reduce the post-operative recovery time and complications. The use of laparoscopic and endoscopic surgical procedures has been relatively popular and has provided additional incentive to develop the procedures further. In laparoscopic procedures, surgery is performed in the interior of the abdomen through a small incision. Similarly, in endoscopic procedures, surgery is performed in any hollow viscus of the body through narrow endoscopic tubes inserted through small entrance wounds in the skin.

[0003] Laparoscopic and endoscopic procedures generally require that the surgical region be insufflated. Accordingly, any instrumentation inserted into the body must be sealed to ensure that gases do not enter or exit the body through the incision. Moreover, laparoscopic and endoscopic procedures often require the surgeon to act on organs, tissues and/or vessels far removed from the incision. Thus, instruments used in such procedures are typically long and narrow while being functionally controllable from a proximal end of the instrument.

[0004] Significant development has gone into a range of endoscopic surgical instruments that are suitable for precise placement of a distal end effector at a desired surgical site through a cannula of a trocar. These distal end effectors engage the tissue in a number of ways to achieve a diagnostic or therapeutic effect (e.g., endocutter, grasper, cutter, staplers, clip applier, access device, drug/gene therapy delivery device, and energy device using ultrasound, RF, laser, etc.).

[0005] Known surgical staplers include an end effector that simultaneously makes a longitudinal incision in tissue and applies lines of staples on opposing sides of the incision. The end effector includes a pair of cooperating jaw members that, if the instrument is intended for endoscopic or laparoscopic applications, are capable of passing through a cannula passageway. One of the jaw members receives a staple cartridge having at least two laterally spaced rows of staples. The other jaw member defines an anvil having staple-forming pockets aligned with the rows of staples in the cartridge. The instrument includes a plurality of reciprocating wedges which, when

driven distally, pass through openings in the staple cartridge and engage drivers supporting the staples to effect the firing of the staples toward the anvil.

[0006] Recently, an improved "E-beam" firing bar was described for a surgical stapling and severing instrument that advantageously included a top pin that slides within an internal slot formed in the upper jaw (anvil) and has a middle pin and bottom foot that slides on opposite sides of a lower jaw of an end effector, or more particularly a staple applying assembly. Distal to the middle pin, a contacting surface actuates a staple cartridge held within an elongate staple channel that forms the lower jaw. Between the contacting surface and the top pin, a cutting surface, or knife, severs tissue clamped between the anvil and the staple cartridge of the lower jaw. Since both jaws are thus engaged by the E-beam, the E-beam maintains a desired spacing between the jaws to ensure proper staple formation. Thus, if a lesser amount of tissue is clamped, the E-beam holds up the anvil to ensure sufficient spacing for the staples to properly form against an undersurface of the anvil. In addition, if a greater amount of tissue is clamped, the E-beam draws down the anvil to ensure that the spacing does not exceed the length of the staple such that ends of each staple are not sufficiently bent to achieve a desired degree of retention. Such an E-beam firing bar is described in U.S. Pat. Appln. No. 10/443,617, entitled "Surgical Stapling Instrument Incorporating an E-Beam Firing Mechanism", filed on May 20, 2003, and in the European Pat. Appln. No. EP-1 479 346-A1.

[0007] While an E-beam firing bar has many advantages for a surgical stapling and severing instrument, often it is desirable to sever and staple tissue of various thicknesses. A thin layer of tissue may result in staples that only form loosely, perhaps requiring the need for bolstering material. A thick layer of tissue may result in formed staples that exert a strong compressive force on the captured tissue, perhaps resulting in necrosis, bleeding or poor staple formation/retention. Rather than limiting the range of tissue thicknesses that are appropriate for a given surgical stapling and severing instrument, it would be desirable to accommodate a wider range of tissue thickness with the same surgical stapling and severing instrument.

[0008] Consequently, a significant need exists for an improved surgical stapling and severing instrument that incorporates a staple applying assembly (end effector) that adjusts to the amount of tissue that is clamped.

BRIEF SUMMARY OF THE INVENTION

[0009] The invention overcomes the above-noted and other deficiencies of the prior art by providing a surgical instrument that incorporates a firing bar as defined by the claims that translates through a staple applying assembly having a lower jaw and a pivotally attached upper jaw, engaging each to assist in maintaining the desired spacing between inner surfaces that compress tissue in

between. Advantageously, the distance between the two jaws is allowed to flex apart slightly to allow for a larger thickness of compressed tissue, yet the firing bar prevents excessive flexure that would exceed the limits on the device to form staples through the compressed tissue. Thereby, enhanced clinical flexibility is achieved with the same surgical instrument being suitable for a larger range of surgical procedures or to accommodate variations in the patient population.

[0010] These and other objects and advantages of the present invention shall be made apparent from the accompanying drawings and the description thereof.

BRIEF DESCRIPTION OF THE FIGURES

[0011] The accompanying drawings, which are incorporated in and constitute a part of this specification, together with the general description of the invention given above, and the detailed description of the embodiments given below, serve to explain the principles of the present invention. Embodiments of the present invention are illustrated in figures 10 - 13.

[0012]

FIG. 1 is a left side view in elevation of a surgical stapling and severing instrument with an open end effector (staple applying assembly) with a shaft partially cut away to expose a firing member of a proximal firing rod and distal firing bar guided by a frame ground and encompassed by a closure sleeve.

FIG. 2 is a left side view of a closed end effector (staple applying assembly) with a retracted force adjusted height firing bar of the surgical stapling and severing instrument of FIG. 1 taken in longitudinal vertical cross section along lines 2-2.

FIG. 3 is a left isometric view of the force adjusted (compliant) height firing bar of FIG. 2.

FIG. 4 is a left side view of a distal portion ("E-beam") of a first version of the force adjusted height firing bar of FIG. 2 having horizontal slits formed respectively between the top pin and cutting surface and between the middle pin and the cutting surface to enhance vertical flexure.

FIG. 5 is a lower left isometric view of a distal portion ("E-beam") of a second version of the force adjusted firing bar of FIG. 2 having a relieved lower area of an upper pin to enhance vertical flexure.

FIG. 6 is a front view in elevation of an upper portion of the E-beam of FIG. 5 taken in vertical and transverse cross section through the upper pin along lines 6-6.

FIG. 7 is a front view of an upper portion of a third version of the E-beam of FIG. 5 taken in vertical and transverse cross section along lines 6-6 but further including relieved upper root attachments of the top pin for enhanced vertical flexure.

FIG. 8 is a front view of an upper portion of a fourth version of the E-beam of FIG. 5 taken in vertical and

transverse cross section along lines 6-6 but including a resilient inner vertical laminate layer instead of a relieved undersurface of the top pin for enhanced vertical flexure.

FIG. 9 is a front view of an upper portion of a fifth version of the E-beam of FIG. 5 taken in vertical and transverse cross section along lines 6-6 but including an upper pin formed of a resilient material instead of a relieved undersurface of the upper pin for enhanced vertical flexure.

FIG. 10 is an upper left isometric view of a distal portion ("E-beam") of a sixth version of the force adjusted firing bar of FIG. 2 having resilient material upon a bottom foot to enhance vertical flexure.

FIG. 11 is a front view in elevation taken in vertical and transverse cross section through the padded lower foot of the end effector (staple applying assembly) of the surgical stapling and severing instrument of FIG. 1.

FIG. 12 is a left view in elevation of a distal portion ("E-beam") of a seventh version of the force adjusted firing bar of FIG. 2 having a proximally and upwardly extended spring arm attached to a lower foot to enhance vertical flexure.

FIG. 13 is a left top isometric view of a distal portion ("E-beam") of an eighth version of the force adjusted firing bar of FIG. 2 having a spring washer encompassing a lower foot to enhance vertical flexure.

DETAILED DESCRIPTION OF THE INVENTION

[0013] Turning to the Drawings, wherein like numerals denote like components throughout the several views, in FIG. 1, a surgical stapling and severing instrument 10 includes a handle portion 12 that is manipulated to position an implement portion 14 including a fastening end effector, depicted as a staple applying assembly 16, distally attached to an elongate shaft 18. The implement portion 14 is sized for insertion through a cannula of a trocar (not shown) for an endoscopic or laparoscopic surgical procedure with an upper jaw (anvil) 20 and a lower jaw 22 of the staple applying assembly 16 closed by depression of a closure trigger 24 toward a pistol grip 26 of the handle portion 12, which advances an outer closure sleeve 28 of the elongate shaft 18 to pivot shut the anvil 20.

[0014] Once inserted into an insufflated body cavity or lumen, the surgeon may rotate the implement portion 14 about its longitudinal axis by twisting a shaft rotation knob 30 that engages across a distal end of the handle 12 and a proximal end of the elongate shaft 18. Thus positioned, the closure trigger 24 may be released, opening the anvil 20 so that tissue may be grasped and positioned. Once satisfied with the tissue held in the staple applying assembly 16, the surgeon depresses the closure trigger 24 until locked against the pistol grip 26, clamping tissue inside of the staple applying assembly 16.

[0015] Then a firing trigger 32 is depressed, drawn to-

ward the closure trigger 24 and pistol grip 26, thereby distally advancing a firing member, depicted as including a proximal firing rod 34 attached to a distal firing bar 36, that is supported within a frame ground 38 that connects the handle portion 12 to the staple applying assembly 16. The firing bar 36 engages an elongate staple channel 40 and actuates a staple cartridge 42 contained therein, both forming the lower jaw 22. The firing bar 36 also engages the closed anvil 20. After releasing the firing trigger 32 to retract the firing bar 36, depression of a closure release button 44 unclamps the closure trigger 24 so that the closure sleeve 28 may be retracted to pivot and open the anvil 20 to release the severed and stapled tissue from the staple applying assembly 16.

[0016] In FIG. 2, the staple applying assembly 16 is closed upon compressed tissue 46. In FIGS. 2-3, the firing bar 36 has a proximal portion 48 that is attached to a distal E-beam 50 that translates within the staple applying assembly 16. As depicted with the firing bar 36 retracted, a vertical portion 52 of the E-beam 50 resides essentially aft of the staple cartridge 42, as after a new staple cartridge 42 has been inserted into the elongate staple channel 40. An upper pin 54 that extends laterally from an upper portion of the vertical portion 52 of the E-beam 50 initially resides within an anvil pocket 56 recessed near a proximal pivoting end of the anvil 20. As the E-beam 50 is distally advanced during firing, the vertical portion 52 passes through a narrow longitudinal anvil slot 58 (FIGS. 1, 11) formed in an undersurface 60 of the anvil 20, a proximally open vertical slot 62 formed in the staple cartridge 42 and an underlying longitudinal channel slot 64 formed in the elongate staple channel 40.

[0017] In FIGS. 2, 11, the narrow longitudinal anvil slot 58 (FIG. 2) communicates upwardly to a laterally widened longitudinal anvil channel 66 sized to slidably receive the upper pin 54. The longitudinal channel slot 64 communicates downwardly to a laterally widened longitudinal channel track 68 that receives a lower foot 70, which is sized to slide therein and is attached at a bottom of the vertical portion 52 of the E-beam 50. A laterally widened middle pin 72 extending from the vertical portion 52 of the E-beam 50 is positioned to slide along a top surface of a bottom tray 74 of the staple cartridge 42, which in turn rests upon the elongate staple channel 40. A longitudinal firing recess 75 formed in the staple cartridge 42 above the bottom tray 74 is sized to allow the middle pin 72 to translate through the staple cartridge 42.

[0018] A distal driving surface 76 of the vertical portion 52 of the E-beam 50 is positioned to translate through the proximally open vertical slot 62 of the staple cartridge 42 and distally drive a wedge sled 78 proximally positioned in the staple cartridge 42. The vertical portion 52 of the E-beam 50 includes a cutting surface 80 along a distal edge above the distal driving surface 76 and below the upper pin 54 that severs the clamped tissue 46 simultaneously with this stapling.

[0019] With particular reference to FIG. 11, it should be appreciated that the wedge sled 78 drives upwardly

staple drivers 82 that in turn drive upwardly staples 83 out of staple apertures 84 formed in a staple body 85 of the staple cartridge 42 to form against the undersurface 60 of the anvil 20 (FIG. 2).

[0020] In FIGS. 2, 11, advantageously, the illustrative spacing, denoted by arrow 86 (FIG. 2), between the upper pin 54 is compliantly biased toward a compressed state wherein 0.015 inches of compressed tissue 46 is contained in the staple applying assembly 16. However, a larger amount of compressed tissue 46 up to about 0.025 inches is allowed by an inherent flexure of the E-beam 50. Excessive flexure, of perhaps up to 0.030 inches, is avoided should the length of staples be insufficient to form with the additional height. It should be appreciated that these dimensions are illustrative for a staple height of 0.036 inches. The same would be true for each category of staple, however.

[0021] In FIG. 4, a first version of a compliant E-beam 50a includes top and bottom horizontal slits 90, 92 from a distal edge of the vertical portion 52a, perhaps formed by electro drilling machine (EDM). The vertical portion 52a thus contains a vertically compliant top distally projecting arm 94 containing the upper pin 54, a knife flange 96 containing the cutting surface 80, and a lower vertical portion 98 containing the distal driving surface 76, middle pin 72 and lower foot 70. The horizontal slits 90, 92 allow a compliant vertical spacing by allowing the top distally arm 94 to pivot upwardly to adjust to increased force from compressed tissue 46 (not shown).

[0022] In FIGS. 5-6, a second version of a compliant E-beam 50b includes left and right lower relieved areas 110, 112 formed into an upper pin 54b to each side of the vertical portion 52, leaving left and right lower bearing points 114, 116 respectively. The outboard position of the bearing points 114, 116 provides a long moment arm to exert the force to flex. It should be appreciated given the benefit of the present disclosure that the dimensions of the relieved areas 110, 112 and the choice of materials for the compliant E-beam 50b may be selected for a desired degree of flexure, given the staple size and other considerations.

[0023] In FIG. 7, a third version of a compliant E-beam 50c is as described above in FIGS. 5-6 with further flexure provided by left and right upper narrow relieved areas 120, 122 formed into opposite top root surfaces of an upper pin 54c proximate to the vertical portion 52.

[0024] In FIG. 8, a fourth version of a compliant E-beam 50d is as described for FIGS. 2-3 with an added feature of a composite/laminate vertical portion 52d that includes a central resilient vertical layer 130 sandwiched between left and right vertical layers 132, 134 that support respectively left and right portions 136, 138 of an upper pin 54d. As the left and right portions 136, 138 are flexed either up or down, the resulting bowing of the left and right vertical layers 132, 134 are accommodated by a corresponding compression or expansion of the central resilient vertical layer 130.

[0025] In FIG. 9, a fifth version of a compliant E-beam

50e is as described for FIGS. 2-3 with an added feature of a discrete upper pin 54e formed of a more flexible material that is inserted through a horizontal aperture 140 through a vertical portion 52e. Thus, left and right outer ends 142, 144 of the discrete upper pin 54e flex in accordance with loading forces.

[0026] Alternatively or in addition to incorporating flexure into an upper pin 54, in FIGS. 10-11, a sixth version of a compliant E-beam 50f as described for FIGS. 2-3, and according to the present invention further includes resilient pads 150 that are attached to upper surfaces 152 of the bottom foot 70. The resilient pads 150 adjust the spacing of the upper pin 54 in accordance to the compression force experienced at the bottom foot 70.

[0027] In FIG. 12, a seventh version of a compliant E-beam 50g is as described above for FIGS. 2-3, and according to the present invention with the added feature of a bottom foot (shoe) 70g having an upwardly aft extended spring finger 160 that resiliently urges the E-beam 50g downwardly to adjust vertical spacing in accordance with loading force.

[0028] In FIG. 13, an eighth version of a compliant E-beam 50h is as described above in FIGS. 2-3, and according to the present invention with the added feature of an oval spring washer 170 resting upon the bottom foot 70 encircling the vertical portion 52 and having an upwardly bowed central portion 172 that resiliently urges the E-beam 50h downwardly to adjust vertical spacing in accordance with loading force.

[0029] While the present invention has been illustrated by description of several embodiments and while the illustrative embodiments have been described in considerable detail, it is not the intention of the applicant to restrict or in any way limit the scope of the appended claims to such detail. Additional advantages and modifications may readily appear to those skilled in the art.

[0030] For example, while a manually operated surgical stapling and severing instrument 10 is depicted for clarity, it should be appreciated that robotically manipulated and/or controlled fastening devices may incorporate a force controlled firing bar.

[0031] For another example, a compliant E-beam consistent with aspects of the present invention may include engagement to an anvil similar to the engagement in the illustrative versions of two structures that slide against opposite sides of the elongate staple channel. Similarly, a compliant E-beam may engage a lower jaw by having a laterally widened portion that slides internally within a channel formed in a lower jaw structure.

[0032] As yet an additional example, in the illustrative version, the staple cartridge 42 is replaceable so that the other portions of the staple applying assembly 16 may be reused. It should be appreciated given the benefit of the present disclosure that applications consistent with the present invention may include a larger disposable portion, such as a distal portion of an elongate shaft and the upper and lower jaws with a staple cartridge permanently engaged as part of the lower jaw.

[0033] As yet another example, the illustrative E-beam advantageously affirmatively spaces the upper and lower jaws from each other. Thus, the E-beam has inwardly engaging surfaces that pull the jaws together during firing in instances where a larger amount of compressed tissue tends to spread the jaws. Thereby the E-beam prevents malformation of staples due to exceeding their effective length. In addition, the E-beam has outwardly engaging surfaces that push the jaws apart during firing in stances where a small amount of tissue or other structure attributes of the instrument tend to pinch the jaws together that may result in staple malformation. Either or both functions may be enhanced by applications consistent with aspects of the invention wherein inherent flexure in the E-beam adjusts to force to allow a degree of closing of the jaws or of opening of the jaws.

Claims

1. A surgical instrument (10), comprising:

an elongate staple channel (40) having a longitudinal channel slot (64) formed therein;
 an anvil (20) pivotally attached to the elongate staple channel to grip tissue and having a staple forming undersurface (60) with a longitudinal anvil slot (58) formed therein;
 a staple cartridge (42) having an upper surface and received in the elongate staple channel and containing a plurality of staples each having a staple length sized for forming a closed staple between a first height and a second height;
 an elongate shaft (18) attached to the staple channel;
 a handle (12) proximally operatively coupled through the elongate shaft to close the anvil and to clamp tissue between the anvil and the staple cartridge to a clamped tissue thickness; and
 a firing bar (36) translated by the handle and received for longitudinal reciprocating motion in the elongate shaft, the firing bar comprising:

a vertical portion (52) passing through the longitudinal anvil slot and the longitudinal channel slot,
 an upper lateral surface (54) extending from the vertical portion positioned to exert an inward compressive force on the anvil during firing translation,
 a lower lateral surface (70) extending from the vertical portion positioned to exert an inward compressive force on the elongate staple channel during firing translation, and

a resilient portion of the firing bar positioned to allow a height between the staple forming undersurface of the anvil and the upper surface of the staple cartridge

to vary between the first and second heights in relation to the clamped tissue thickness, **characterized in that** the surgical instrument further comprises a resilient member (150, 160, 170) attached to an inner surface of a selected one of a group consisting of the upper lateral surface and the lower lateral surface.

Patentansprüche

1. Chirurgisches Instrument (10) umfassend:

einen langgestreckten Klammernkanal (40) mit einer darin geformten, längs verlaufenden Kanalnut (64);
 einem am langgestreckten Klammernkanal schwenkbar angebrachten Amboss (20) zum Greifen von Gewebe, der eine klammerformende Unterfläche (60) aufweist, in die eine Ambosslängsnut (58) geformt ist;
 ein in dem langgestreckten Klammernkanal aufgenommenes Klammernmagazin (42) mit einer oberen Fläche, das eine Vielzahl von Klammern enthält, von denen jede eine auf das Bilden einer zwischen einer ersten Höhe und einer zweiten Höhe geschlossenen Klammer zugeschnittene Länge hat;
 einen am Klammernkanal angebrachten langgestreckten Schaft (18);
 einen über den langgestreckten Schaft proximal bedienbar verbundenen Griff (12) zum Schließen des Ambosses und zum Klammern von Gewebe zwischen dem Amboss und dem Klammernmagazin auf eine Dicke geklammerten Gewebes; und
 eine von dem Griff verschobene und zur Hin- und Herbewegung in Längsrichtung in dem langgestreckten Schaft aufgenommene Auswurfstange (36), umfassend:

einen durch die Ambosslängsnut und die längs verlaufende Kanalnut verlaufenden vertikalen Abschnitt (52),
 eine sich von dem vertikalen Abschnitt erstreckende obere seitliche Fläche (54), die zum Ausüben einer inwärtigen Druckkraft auf den Amboss während Auswurftranslation positioniert ist,
 eine sich von dem vertikalen Abschnitt erstreckende untere seitliche Fläche (70), die zum Ausüben einer inwärtigen Druckkraft auf den langgestreckten Klammernkanal während Auswurftranslation positioniert ist, und
 einen nachgiebigen Abschnitt der Auswurfstange, die positioniert ist zum Ermöglichen des Variierens einer Höhe zwischen der ei-

ne Klammer bildenden Unterfläche des Ambosses und der oberen Fläche des Klammernmagazins zwischen der ersten und der zweiten Höhe in Bezug auf die Dicke des geklammerten Gewebes, **dadurch gekennzeichnet, dass** das chirurgische Instrument ferner ein nachgiebiges Glied (150, 160, 170), das an eine innere Fläche einer Auswahl aus einer aus der oberen seitlichen Fläche und der unteren seitlichen Fläche bestehenden Gruppe, befestigt ist, umfasst.

Revendications

1. Instrument chirurgical (10), comprenant :

> un canal d'agrafes oblong (40) présentant une fente de canal longitudinal (64) formée dans celui-ci ;
 > une enclume (20) fixée de manière pivotante au canal d'agrafes oblong pour saisir le tissu et présentant une surface inférieure formant agrafe (60) avec une fente d'enclume longitudinale (58) formée dans celle-ci ;
 > une cartouche d'agrafes (42) présentant une surface supérieure et reçue dans le canal d'agrafes oblong et contenant une pluralité d'agrafes ayant chacune une longueur d'agrafe dimensionnée pour former une agrafe fermée entre une première hauteur et une seconde hauteur ;
 > une tige oblongue (18) fixée au canal d'agrafes ;
 > une poignée (12) couplée opérationnellement de manière proximale par le biais de la tige oblongue pour fermer l'enclume et serrer le tissu entre l'enclume et la cartouche d'agrafes à une épaisseur de tissu serré ; et
 > une barre de déclenchement (36) déplacée en translation grâce à la poignée et reçue pour effectuer un mouvement de va-et-vient longitudinal dans la tige oblongue, la barre de déclenchement comprenant :

> une partie verticale (52) passant à travers la fente d'enclume longitudinale et la fente de canal longitudinal,
 > une surface latérale supérieure (54) s'étendant depuis la partie verticale positionnée pour exercer une force de compression vers l'intérieur sur l'enclume au cours de la translation de déclenchement,
 > une surface latérale inférieure (70) s'étendant de la partie verticale positionnée de manière à exercer une force de compression vers l'intérieur sur le canal d'agrafes

oblong au cours de la translation de déclenchement, et

> une partie résiliente de la barre de déclenchement positionnée pour permettre à une hauteur entre la surface inférieure formant agrafe de l'enclume et la surface supérieure de la cartouche d'agrafes de varier entre les première et seconde hauteurs en fonction de l'épaisseur du tissu serré, **caractérisé en ce que** l'instrument chirurgical comprend en outre un élément résilient (150, 160, 170) fixé à une surface interne d'une surface choisie dans un groupe constitué de la surface latérale supérieure et de la surface latérale inférieure.

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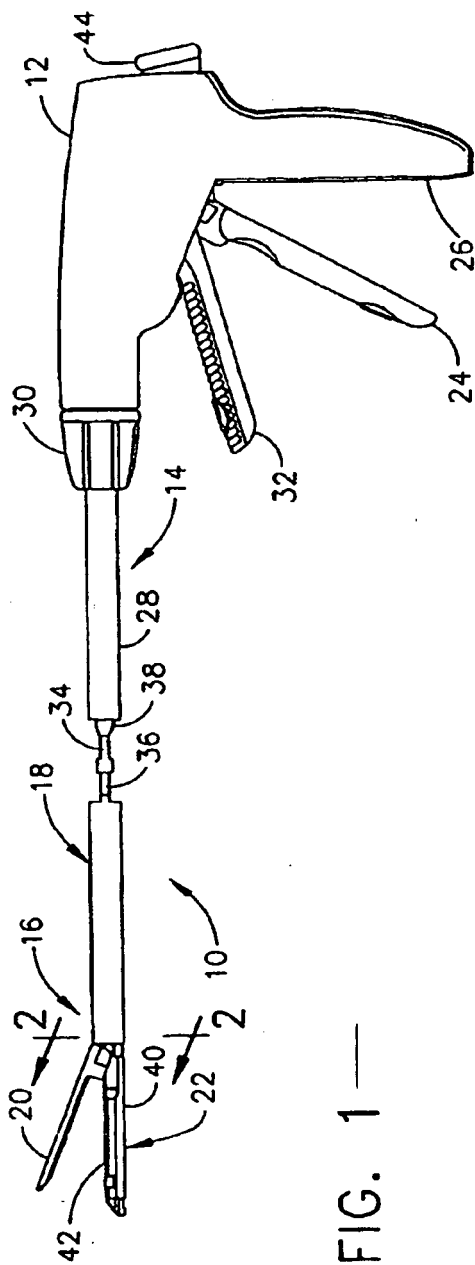


FIG. 1 —

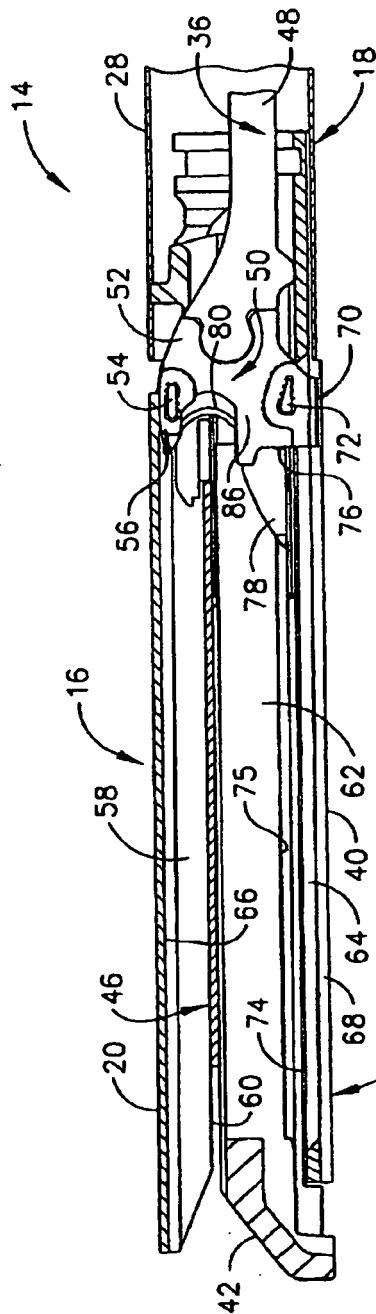


FIG. 2

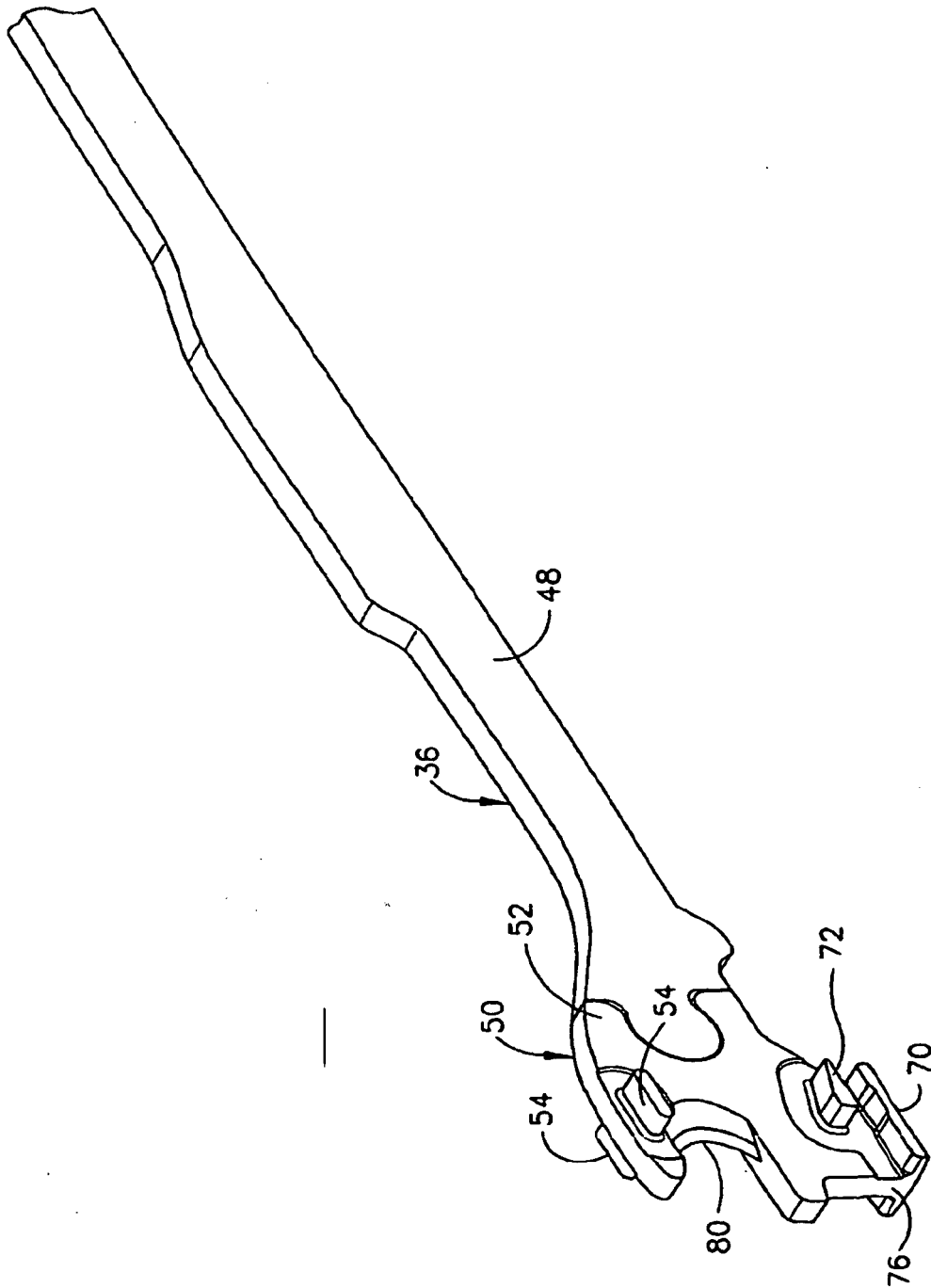


FIG. 3

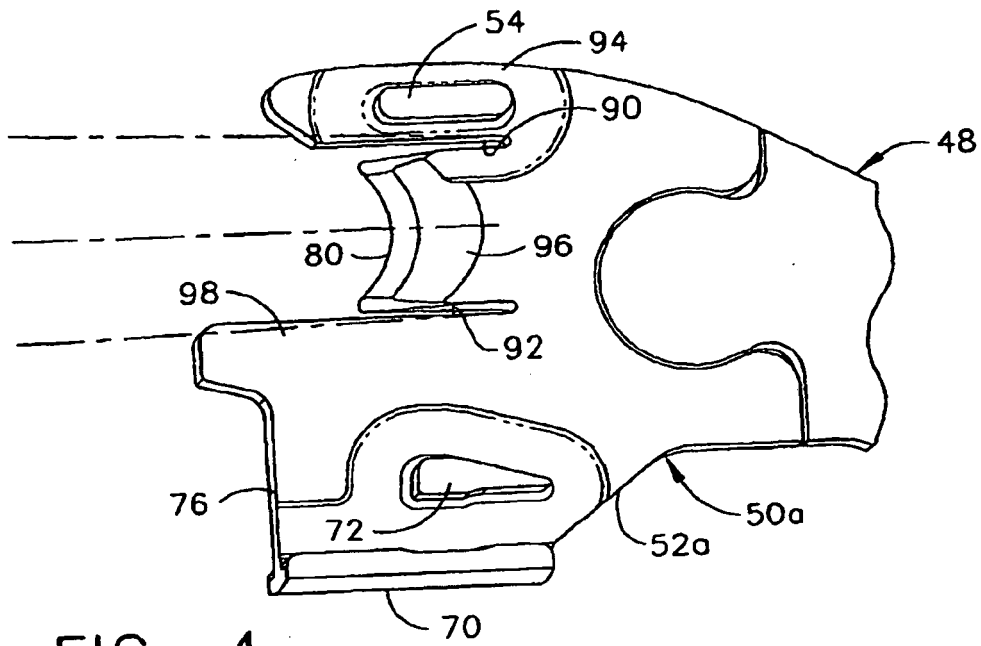


FIG. 4

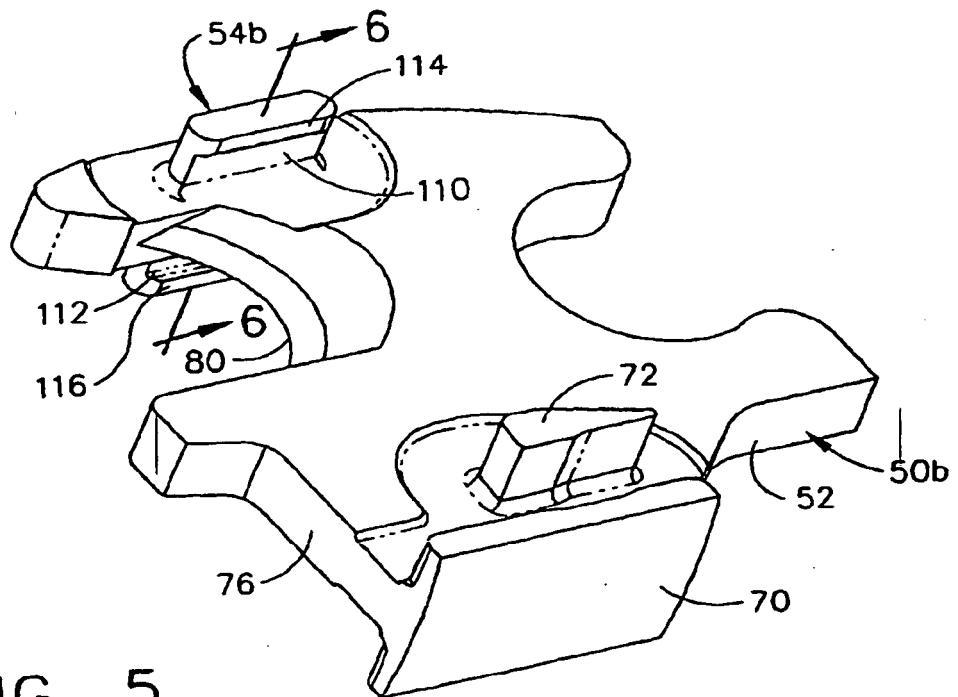


FIG. 5

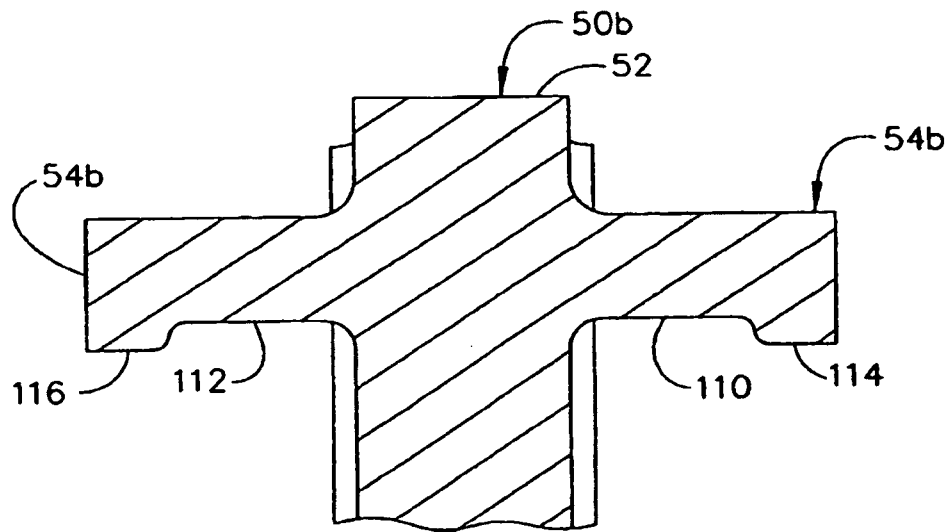


FIG. 6

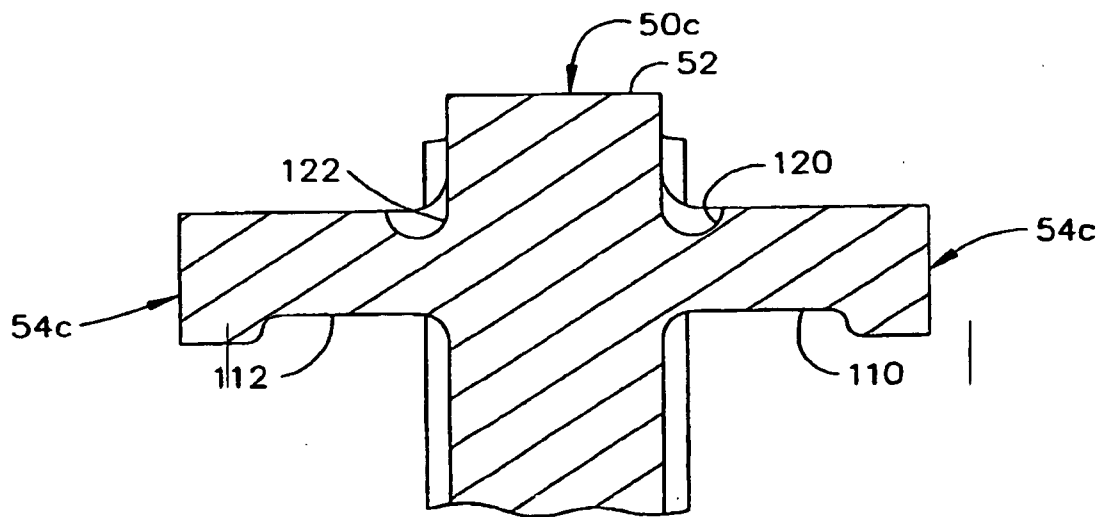


FIG. 7

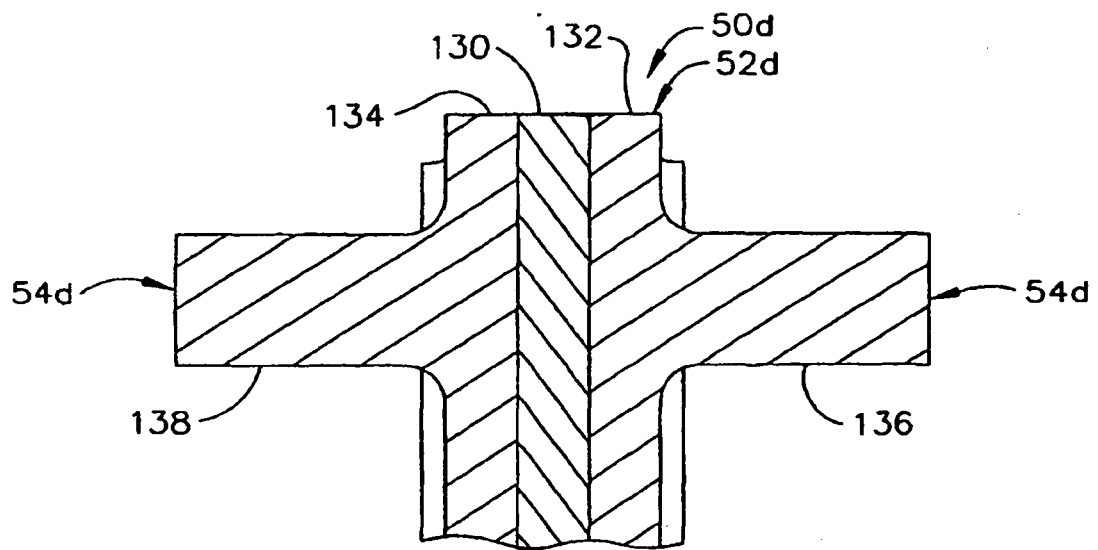


FIG. 8

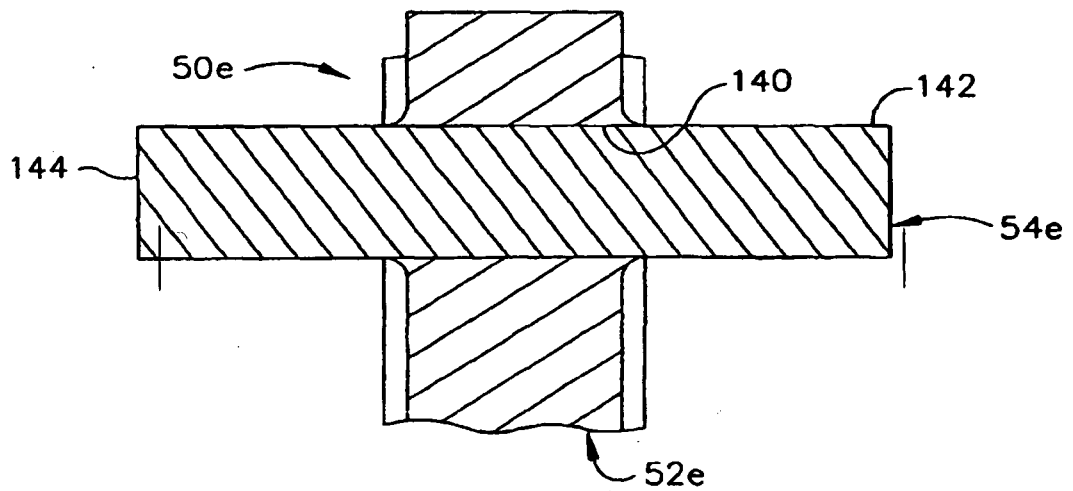


FIG. 9

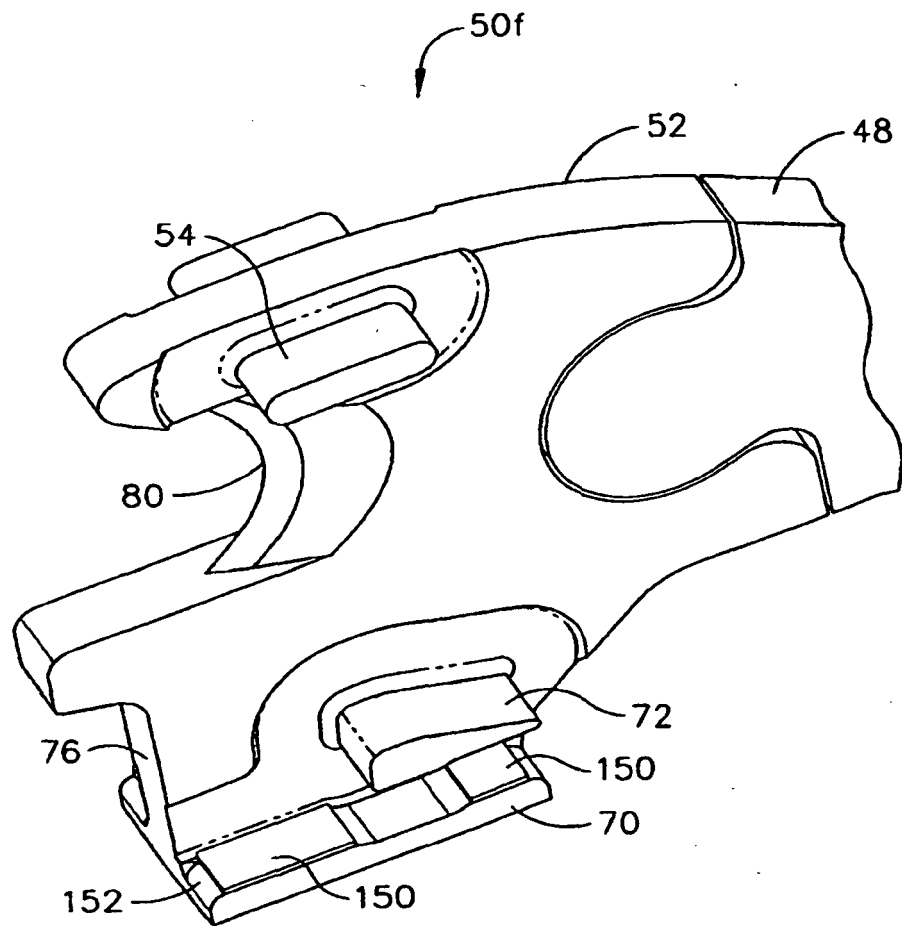


FIG. 10

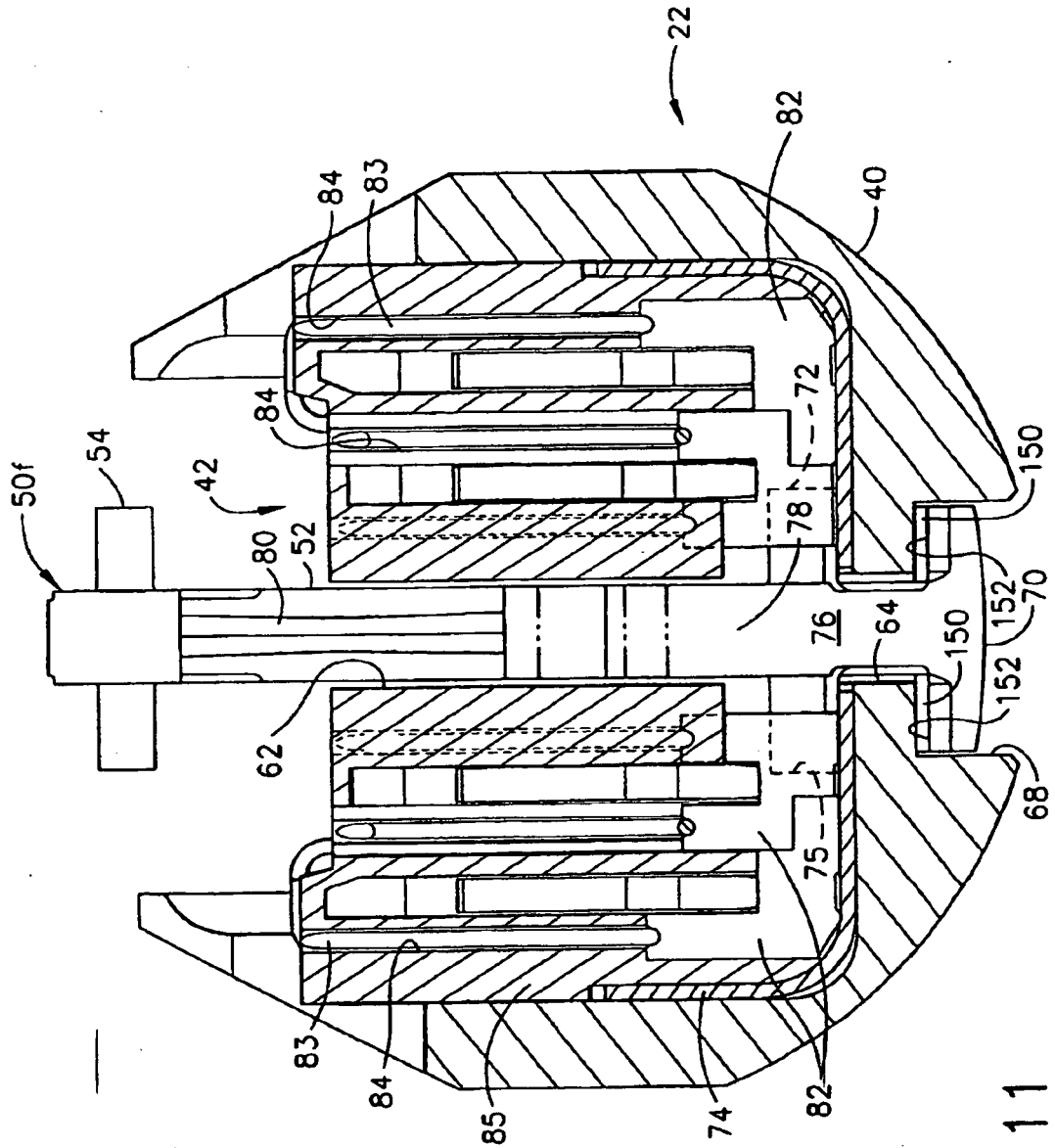
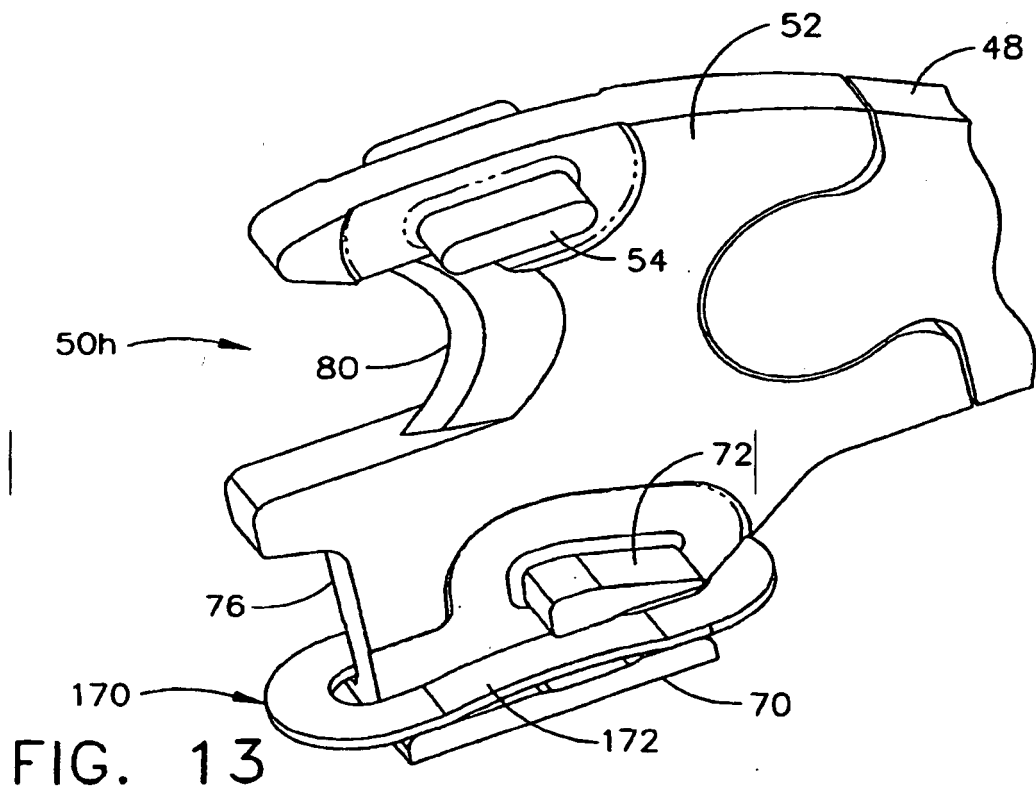
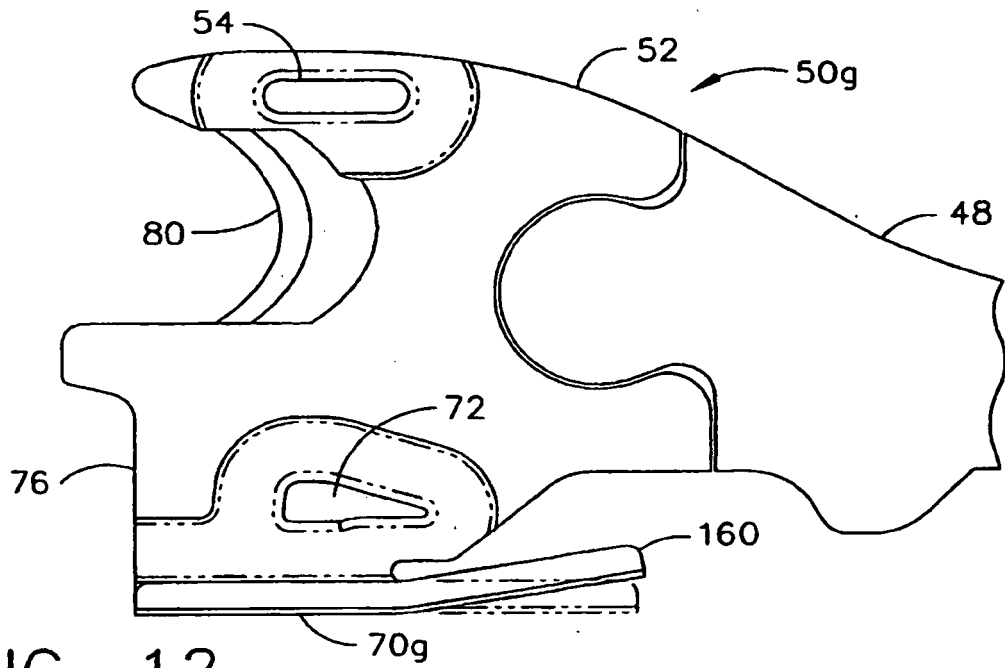


FIG. 11



REFERENCES CITED IN THE DESCRIPTION

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- US 44361703 A [0006]
- EP 1479346 A1 [0006]

专利名称(译)	具有受力控制的间隔末端执行器的外科缝合器械		
公开(公告)号	EP1767156B2	公开(公告)日	2017-06-21
申请号	EP2006254867	申请日	2006-09-20
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IPC分类号	A61B17/072 A61B17/00		
CPC分类号	A61B17/07207 A61B90/03 A61B2017/0725 A61B2017/07278 A61B2017/07285 A61B2017/320052		
优先权	11/231456 2005-09-21 US		
其他公开文献	EP1767156A1 EP1767156B1		
外部链接	Espacenet		

摘要(译)

用于内窥镜或腹腔镜插入手术部位以同时缝合和切断组织的手术器械包括上颌或砧座（20）与下颌之间的力调节间隔，下颌包括与细长钉通道接合的钉仓（42）（40）使得订书钉形成的高度对应于组织的厚度，但是不超过钉的长度可以容纳的高度范围。特别地，弹性结构形成为电子束击发杆（50），其包括切割表面或刀（80），该切割表面或刀（80）在与砧座接合的顶销（54）和中间销（72）之间切断组织（46）。并且下脚（70）与下颌接合。弹性响应于被夹紧的组织施加的力以改变间距。

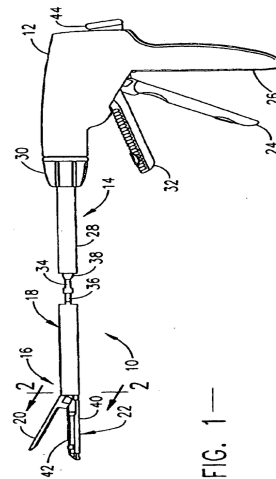


FIG. 1—

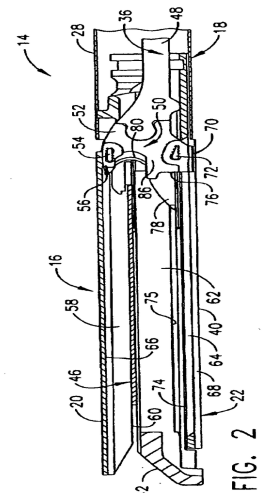


FIG. 2