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(54) **Surgical stapling instrument having a spent cartridge lockout**

Chirurgisches Klammergerät mit bei einer verbrauchten Patrone aktivierter Sperrvorrichtung

Agrafeuse chirurgicale avec moyens de blocage d'une cartouche utilisée

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Description

Field of the Invention

[0001] The present invention relates in general to surgical stapler instruments that are capable of applying lines of staples to tissue while cutting the tissue between those staple lines and, more particularly, to improvements relating to stapler instruments and improvements in processes for forming various components of such stapler instruments.

Background of the Invention

[0002] Surgical staplers have been used in the prior art to simultaneously make a longitudinal incision in tissue and apply lines of staples on opposing sides of the incision. Such instruments commonly include a pair of cooperating jaw members that, if the instrument is intended for endoscopic or laparoscopic applications, are capable of passing through a cannula passageway. One of the jaw members receives a staple cartridge having at least two laterally spaced rows of staples. The other jaw member defines an anvil having staple-forming pockets aligned with the rows of staples in the cartridge. The instrument includes a plurality of reciprocating wedges which, when driven distally, pass through openings in the staple cartridge and engage drivers supporting the staples to effect the firing of the staples toward the anvil.

[0003] An example of a surgical stapler suitable for endoscopic applications is described in U.S. Pat. No. 5,465,895, which advantageously provides distinct closing and firing actions. Thereby, a clinician is able to close the jaw members upon tissue to position the tissue prior to firing. Once the clinician has determined that the jaw members are properly gripping tissue, the clinician can then fire the surgical stapler, thereby severing and stapling the tissue. The simultaneous severing and stapling avoids complications that may arise when performing such actions sequentially with different surgical tools that respectively only sever or staple.

[0004] It is often advantageous to build an end effector for the surgical stapler that is reusable. For instance, one patient may need a series of severing and stapling operations. Replacing an entire end effector for each operation tends to be economically inefficient. This is especially true if the end effector is built to be strong and reliable over repeated operations. To that end, staple cartridges are fitted into the end effector prior to each operation of the surgical stapler. Thus, a much smaller amount of the surgical stapler is discarded after each use.

[0005] While the staple cartridge provides numerous advantages, it is desirable to prevent inadvertent firing of the surgical stapler when a spent staple cartridge is installed. Otherwise, the severing of tissue may occur without the staples to minimize bleeding. US patent 6 109 500 and patent application WO 03/030743 each disclose a surgical stapler having a reciprocating firing drive

means provided with a locking member coupled and articulated thereto, and disabled before firing by a part of the cartridge wall.

[0006] It is particularly desirable that preventing such inadvertent firing be accomplished in a reliable way that is not subject to an intervening malfunction. Moreover, for ease of manufacturing and assembly, it is further desirable that the lockout features be accomplished with a minimum number of components.

[0007] Consequently, a significant need exists for an improved surgical stapling and severing instrument that prevents inadvertent firing (i.e., severing and stapling) when a staple cartridge is not installed or is spent, having been previously fired.

Brief Summary of the Invention

[0008] The invention overcomes the above-noted and other deficiencies of the prior art by providing a lockout mechanism that prevents firing a surgical stapling and severing instrument when a staple cartridge is already spent. In particular, the lock mechanism prevents distal movement of a firing bar, and thus severing of tissue, in instances where simultaneous stapling would not occur.

[0009] For use with the cartridge of the invention, a surgical instrument includes a handle portion operable to produce a firing motion that actuates an implement portion. This implement portion has an elongate channel that receives a staple cartridge with a firing drive slot defined therein. A firing mechanism engages the firing drive slot along its longitudinal length and includes an engaging device that traverses the firing drive slot for distally moving a wedge sled in the staple cartridge. A lockout mechanism is advantageously positioned to be moved out of the firing drive slot by the presence of the wedge sled in its unfired, proximal position, and thus allowing the firing bar to fire. When the wedge sled is moved to its distal position (i.e., spent cartridge), the lockout mechanism resiliently moves downwardly from the staple cartridge into the firing drive slot. The proximal and distal sides of the lockout mechanism present in the firing drive slot are shaped to allow the engaging device of the firing bar to return to its proximal, initial position but to thereafter impede distal movement until an unfired staple cartridge is installed.

[0010] These and other objects and advantages of the present invention shall be made apparent from the accompanying drawings and the description thereof. A cartridge according to the invention is defined in appended claim 1. Further preferred features thereof are defined in subclaims 2-4. A surgical instrument comprising the cartridge of the invention is defined in appended claim 5. Further preferred features thereof are defined in subclaims 6-7.

Brief Description of the Figures

[0011] The accompanying drawings, which are incor-

porated in and constitute a part of this specification, illustrate embodiments of the invention, and, together with the general description of the invention given above, and the detailed description of the embodiments given below, serve to explain the principles of the present invention.

[0012] FIG. 1 depicts a partially cut-away side elevation view of a surgical stapling and severing instrument in an open position.

[0013] FIG. 2 depicts a cross-sectional side elevation detail view along the line 2-2 of FIG. 1 of an end effector of the surgical stapling and severing instrument.

[0014] FIG. 3 depicts an enlarged side elevation view of the firing bar of the surgical stapling and severing instrument of FIG. 2.

[0015] FIG. 4 depicts an enlarged front view of the firing bar of the surgical stapling and severing instrument of FIG. 2.

[0016] FIG. 5 depicts a cross-sectional side elevation detail view of an alternative end effector for the surgical stapling and severing instrument of FIG. 1, incorporating a firing bar that lacks a middle pin for preventing pinching of the end effector.

[0017] FIG. 6 depicts a side elevational view of a handle portion of a proximal end of the surgical stapling and severing instrument of FIG. 1 with a left side removed to expose interior parts in an unclamped, unfired ("start") position.

[0018] FIG. 7 depicts a perspective, exploded view of the handle portion of the proximal end of the surgical stapling and severing instrument of FIG. 1.

[0019] FIG. 8 depicts a side elevational view of the handle portion of the proximal end of the surgical stapling and severing instrument of FIG. 1 with the left side removed to expose interior parts in the closed ("clamped") position.

[0020] FIG. 9 depicts a side elevational view of the handle portion of proximal end of surgical stapling and severing instrument of FIG. 1 with the left side removed to expose interior parts in the stapled and severed ("fired") position.

[0021] FIG. 10 depicts an isometric view of the end effector at the distal end of the surgical stapling and severing instrument of FIG. 1 with the anvil in the up or open position exposing the staple cartridge and cutting edge of the firing bar.

[0022] FIG. 11 depicts an isometric, exploded view of the implement portion of the surgical stapling and severing instrument of FIG. 1.

[0023] FIG. 12 depicts an isometric view of the end effector at the distal end of the surgical stapling and severing instrument of FIG. 1 with the anvil in the up or open position with the cartridge largely removed exposing a single staple driver and a double staple driver as exemplary and the wedge sled in its start position against a middle pin of the firing bar.

[0024] FIG. 13 depicts an isometric view of the distal end of the surgical stapling and severing instrument of FIG. 1 with the anvil in the up or open position with the

staple cartridge completely removed and a portion of an elongate channel removed to expose a lowermost pin of the firing bar.

[0025] FIG. 14 depicts a side elevation view in section showing a mechanical relationship between the anvil, elongate channel, and staple cartridge in the closed position of the surgical stapling and severing instrument of FIG. 1, the section generally taken along lines 14-14 of FIG. 10 to expose wedge sled, staple drivers and staples but also depicting the firing bar along the longitudinal centerline.

[0026] FIG. 15 depicts a section view of the end effector of the surgical stapling and severing instrument with the cartridge and firing bar in the start position taken along line 15-15 of FIG. 10.

[0027] FIG. 16 depicts a section view taken along line 16-16 of FIG. 15 showing the cross-sectional relationship between the firing bar, elongate channel, wedge sled, staple drivers, staples and staple cartridge.

[0028] FIG. 17 depicts a side elevation section view of the surgical stapling and severing instrument of FIG. 1 taken along the longitudinal centerline of the end effector in a partially closed but unclamped position gripping tissue.

[0029] FIG. 18 depicts a partially cut-away side elevational view of the surgical stapling and severing instrument of FIG. 1 in the closed or clamped position.

[0030] FIG. 19 depicts a side elevation view in centerline section of the distal end of the surgical stapling and severing instrument of FIG. 1 in the closed or clamped position with tissue properly compressed.

[0031] FIG. 20 depicts a partially cut-away side elevation view of the surgical stapling and severing instrument of FIG. 1 in a partially fired position.

[0032] FIG. 21 depicts a view in centerline section of the distal end of the surgical stapling and severing instrument of FIG. 1 in a partially fired position.

[0033] FIG. 22 depicts a partially cut-away side elevation view of the surgical stapling and severing instrument of FIG. 1 in a fully fired position.

[0034] FIG. 23 depicts a view in centerline section of the distal end of the surgical stapling and severing instrument of FIG. 1 in a fully fired position.

[0035] FIG. 24 depicts a perspective bottom view looking distally at the elongate channel partially cut away to expose part of a cartridge body and a spent cartridge lockout mechanism engaging a middle pin of a firing bar.

[0036] FIGS. 25-28 depict a cross-sectional side detail view of the spent cartridge lockout mechanism, staple cartridge and firing bar of FIG. 24, sequentially shown in a cartridge loaded and unfired state in FIG. 25, a cartridge being fired state in FIG. 26, a spent cartridge with firing bar being retracted state in FIG. 27, and spent cartridge with firing bar retracted state in FIG. 28.

[0037] FIG. 29 depicts a bottom perspective view of a partially cut-away cartridge body to expose an integral spent cartridge lockout mechanism.

[0038] FIGS. 30-33 depict a cross-sectional side detail

view of the integral spent cartridge lockout mechanism of FIG. 29, sequentially shown in a cartridge loaded and unfired state in FIG. 30, a cartridge being fired state in FIG. 31, a spent cartridge with firing bar being retracted state in FIG. 32, and a spent cartridge with firing bar retracted state in FIG. 33.

Detailed Description of the Invention

[0039] Turning to the Drawings, wherein like numerals denote like components throughout the several views, FIG. 1 and 2 depict a surgical stapling and severing instrument 10 that is capable of practicing the unique benefits of the present invention. The surgical stapling and severing instrument 10 incorporates an end effector 12 having an E-beam firing mechanism ("firing bar") 14 that advantageously controls the spacing of the end effector 12. In particular, an elongate channel 16 and a pivotally translatable anvil 18 are maintained at a spacing that assures effective stapling and severing. Furthermore, firing (i.e., severing and stapling) is prevented from occurring if the instrument is not capable of stapling with a single lockout mechanism, which is described in more detail below.

[0040] The surgical and stapling and severing instrument 10 includes a handle portion 20 connected to an implement portion 22, the latter further comprising a shaft 23 distally terminating in the end effector 12. The handle portion 20 includes a pistol grip 24 toward which a closure trigger 26 is pivotally drawn by the clinician to cause clamping, or closing, of the anvil 18 toward the elongate channel 16 of the end effector 12. A firing trigger 28 is farther outboard of the closure trigger 26 and is pivotally drawn by the clinician to cause the stapling and severing of clamped tissue in the end effector 12.

[0041] It will be appreciated that the terms "proximal" and "distal" are used herein with reference to a clinician gripping a handle of an instrument. Thus, the end effector 12 is distal with respect to the more proximal handle portion 20. It will be further appreciated that for convenience and clarity, spatial terms such as "vertical" and "horizontal" are used herein with respect to the drawings. However, surgical instruments are used in many orientations and positions, and these terms are not intended to be limiting and absolute.

[0042] Closure trigger 26 is actuated first. Once the clinician is satisfied with the positioning of the end effector 12, the clinician may draw back the closure trigger 26 to its fully closed, locked position proximate to the pistol grip 24. Then, the firing trigger 28 is actuated. The firing trigger 28 springedly returns when the clinician removes pressure. A release button 30 when depressed on the proximal end of the handle portion 20 releases any locked closure trigger 26.

[0043] A closure sleeve 32 encloses a frame 34, which in turn encloses a firing drive member 36 that is positioned by the firing trigger 28. The frame 34 connects the handle portion 20 to the end effector 12. With the closure

sleeve 32 withdrawn proximally by the closure trigger 26 as depicted, the anvil 18 springedly opens, pivoting away from the elongate channel 16 and translating proximally with the closure sleeve 32.

[0044] The elongate channel 16 receives a staple cartridge 37 that is responsive to the firing bar 14 to drive staples into forming contact with the anvil 18. It will be appreciated that although a readily replaceable staple cartridge 37 is advantageously described herein, a staple cartridge 37 consistent with aspects of the present invention may be permanently affixed or integral to the elongate channel 16, for instance when a larger portion of the end effector 12 is replaced after each firing.

[0045] E-BEAM FIRING MECHANISM

[0046] With particular reference to FIGS. 2-4, the firing bar 14 includes three vertically spaced pins that control the spacing of the end effector 12 during firing. In particular, an upper pin 38 is staged to enter an anvil pocket 40 near the pivot between the anvil 18 and elongate channel 16. When fired with the anvil 18 closed, the upper pin 38 advances distally within a longitudinal anvil slot 42 extending distally through anvil 18. Any minor upward deflection in the anvil 18 is overcome by a downward force imparted by the upper pin 38.

[0047] Firing bar 14 also includes a lower most pin, or firing bar cap, 44 that upwardly engages a channel slot 45 in the elongate channel 16, thereby cooperating with the upper pin 38 to draw the anvil 18 and the elongate channel 16 slightly closer together in the event of excess tissue clamped therebetween.

[0048] The firing bar 14 advantageously includes a middle pin 46 that passes through a firing drive slot 47 formed in a lower surface of the cartridge 37 and an upward surface of the cartridge tray 224, thereby driving the staples therein as described below. The middle pin 46, by sliding against the cartridge tray 224, advantageously resists any tendency for the end effector 12 to be pinched shut at its distal end. To illustrate an advantage of the middle pin 46, FIG. 5 depicts an alternative end effector 12' that lacks a middle pin on a firing bar 14'. In this depiction, the end effector 12' is allowed to pinch shut at its distal end, which tends to impair desired staple formation.

[0049] Returning to FIGS. 2-4, a distally presented cutting edge 48 between the upper and middle pins 38, 46 on the firing bar 14 traverses through a proximally presented, vertical slot 49 in the cartridge 37 to sever clamped tissue. The affirmative positioning of the firing bar 14 with regard to the elongate channel 16 and anvil 18 assure that an effective cut is performed.

CAMBERED ANVIL WITH SELECTED CARTRIDGE GAP

[0050] The affirmative vertical spacing provided by the E-Beam firing bar 14 is suitable for the limited size available for endoscopic devices. Moreover, the E-Beam firing bar 14 enables fabrication of an anvil 16 with a camber

imparting a vertical deflection at its distal end, similar to the position depicted in FIG. 5. This cambered anvil 16 advantageously assists in achieving the desired gap in the end effector 12 even with an anvil 16 reduced thickness, which is thus more suited to the size limitations of an endoscopic device.

[0051] The E-Beam firing bar 14 further enables increased applications, especially in combination with a range of configurations of staple cartridges. For instance, a clinician may select a gray staple cartridge yielding a 0.02 mm tissue gap, a white staple cartridge yielding a 0.04 mm tissue gap, a blue cartridge yielding a 0.06 mm tissue gap, or a green cartridge yielding a 0.10 mm tissue gap. The vertical height of each respective staple cartridge in combination with the length of staples and an integral wedge sled (described in more detail below) pre-determines this desired tissue thickness with the anvil 18 appropriately vertically spaced by the E-Beam firing bar 14.

TWO-AXIS HANDLE

[0052] With reference to FIGS. 6-9, the handle portion 20 is comprised of first and second base sections 50 and 52, which are molded from a polymeric material such as a glass-filled polycarbonate. The first base section 50 is provided with a plurality of cylindrical-shaped pins 54. The second base section 52 includes a plurality of extending members 56, each having a hexagonal-shaped opening 58. The cylindrical-shaped pins 54 are received within the hexagonal-shaped openings 58 and are frictionally held therein for maintaining the first and second base sections 50 and 52 in assembly.

[0053] A rotating knob 60 has a bore 62 extending completely through it for engaging and rotating the implement portion 22 about its longitudinal axis. The rotating knob 60 includes an inwardly protruding boss 64 extending along at least a portion of the bore 62. The protruding boss 64 is received within a longitudinal slot 66 formed at a proximal portion of the closure sleeve 32 such that rotation of the rotating knob 60 effects rotation of the closure sleeve 32. It will be appreciated that the boss 64 further extends through frame 34 and into contact with a portion of the firing drive member 36 to effect their rotation as well. Thus, the end effector 12 (not shown in FIGS. 6-9) rotates with the rotating knob 60.

[0054] A proximal end 68 of the frame 34 passes proximally through the rotating knob 60 and is provided with a circumferential notch 70 that is engaged by opposing channel securement members 72 extending respectively from the base sections 50 and 52. Only the channel securement member 72 of the second base section 52 is shown. The channel securement members 72 extending from the base sections 50, 52 serve to secure the frame 34 to the handle portion 20 such that the frame 34 does not move longitudinally relative to the handle portion 20.

[0055] The closure trigger 26 has a handle section 74, a gear segment section 76, and an intermediate section

78. A bore 80 extends through the intermediate section 78. A cylindrical support member 82 extending from the second base section 52 passes through the bore 80 for pivotally mounting the closure trigger 26 on the handle portion 20. A second cylindrical support member 83 extending from the second base section 52 passes through a bore 81 of firing trigger 28 for pivotally mounting on the handle portion 20. A hexagonal opening 84 is provided in the cylindrical support member 83 for receiving a securement pin (not shown) extending from the first base section 50.

[0056] A closure yoke 86 is housed within the handle portion 20 for reciprocating movement therein and serves to transfer motion from the closure trigger 26 to the closure sleeve 32. Support members 88 extending from the second base section 52 and securement member 72, which extends through a recess 89 in the yoke 86, support the yoke 86 within the handle portion 20.

[0057] A proximal end 90 of the closure sleeve 32 is provided with a flange 92 that is snap-fitted into a receiving recess 94 formed in a distal end 96 of the yoke 86. A proximal end 98 of the yoke 86 has a gear rack 100 that is engaged by the gear segment section 76 of the closure trigger 26. When the closure trigger 26 is moved toward the pistol grip 24 of the handle portion 20, the yoke 86 and, hence, the closure sleeve 32 move distally, compressing a spring 102 that biases the yoke 86 proximally. Distal movement of the closure sleeve 32 effects pivotal translation movement of the anvil 18 distally and toward the elongate channel 16 of the end effector 12 and proximal movement effects closing, as discussed below.

[0058] The closure trigger 26 is forward biased to an open position by a front surface 130 interacting with an engaging surface 128 of the firing trigger 28. Clamp first hook 104 that pivots top to rear in the handle portion 20 about a pin 106 restrains movement of the firing trigger 28 toward the pistol grip 24 until the closure trigger 26 is clamped to its closed position. Hook 104 restrains firing trigger 28 motion by engaging a lockout pin 107 in firing trigger 28. The hook 104 is also in contact with the closure trigger 26. In particular, a forward projection 108 of the hook 104 engages a member 110 on the intermediate section 78 of the closure trigger 26, the member 110 being outward of the bore 80 toward the handle section 74. Hook 104 is biased toward contact with member 110 of the closure trigger 26 and engagement with lockout pin 107 in firing trigger 28 by a release spring 112. As the closure trigger 26 is depressed, the hook 104 is moved top to rear, compressing the release spring 112 that is captured between a rearward projection 114 on the hook 104 and a forward projection 116 on the release button 30.

[0059] As the yoke 86 moves distally in response to proximal movement of the closure trigger 26, an upper latch arm 118 of the release button 30 moves along an upper surface 120 on the yoke 86 until dropping into an upwardly presented recess 122 in a proximal, lower por-

tion of the yoke 86. The release spring 112 urges the release button 30 outward, which pivots the upper latch arm 118 downwardly into engagement with the upwardly presented recess 122, thereby locking the closure trigger 26 in a tissue clamping position, such as depicted in FIG. 8.

[0060] The latch arm 118 can be moved out of the recess 122 to release the anvil 18 by pushing the release button 30 inward. Specifically, the upper latch arm 118 pivots upward about pin 123 of the second base section 52. The yoke 86 is then permitted to move proximally in response to return movement of the closure trigger 26.

[0061] A firing trigger return spring 124 is located within the handle portion 20 with one end attached to pin 106 of the second base section 52 and the other end attached to a pin 126 on the firing trigger 28. The firing return spring 124 applies a return force to the pin 126 for biasing the firing trigger 28 in a direction away from the pistol grip 24 of the handle portion 20. The closure trigger 26 is also biased away from pistol grip 24 by engaging surface 128 of firing trigger 28 biasing front surface 130 of closure trigger 26.

[0062] As the closure trigger 26 is moved toward the pistol grip 24, its front surface 130 engages with the engaging surface 128 on the firing trigger 28 causing the firing trigger 28 to move to its "firing" position. When in its firing position, the firing trigger 28 is located at an angle of approximately 45° to the pistol grip 24. After staple firing, the spring 124 causes the firing trigger 28 to return to its initial position. During the return movement of the firing trigger 28, its engaging surface 128 pushes against the front surface 130 of the closure trigger 26 causing the closure trigger 26 to return to its initial position. A stop member 132 extends from the second base section 52 to prevent the closure trigger 26 from rotating beyond its initial position.

[0063] The surgical stapling and severing instrument 10 additionally includes a reciprocating section 134, a multiplier 136 and a drive member 138. The reciprocating section 134 comprises a wedge sled in the implement portion 22 (not shown in FIG. 6-9) and a metal drive rod 140.

[0064] The drive member 138 includes first and second gear racks 141 and 142. A first notch 144 is provided on the drive member 138 intermediate the first and second gear racks 141, 142. During return movement of the firing trigger 28, a tooth 146 on the firing trigger 28 engages with the first notch 144 for returning the drive member 138 to its initial position after staple firing. A second notch 148 is located at a proximal end of the metal drive rod 140 for locking the metal drive rod 140 to the upper latch arm 118 of the release button 30 in its unfired position.

[0065] The multiplier 136 comprises first and second integral pinion gears 150 and 152. The first integral pinion gear 150 is engaged with a first gear rack 154 provided on the metal drive rod 140. The second integral pinion gear 152 is engaged with the first gear rack 141 on the drive member 138. The first integral pinion gear 150 has

a first diameter and the second integral pinion gear 152 has a second diameter which is smaller than the first diameter.

[0066] FIGS. 6, 8 and 9 depict respectively the handle portion 20 in the start position (open and unfired), a clamped position (closed and unfired) and a fired position. The firing trigger 28 is provided with a gear segment section 156. The gear segment section 156 engages with the second gear rack 142 on the drive member 138 such that motion of the firing trigger 28 causes the drive member 138 to move back and forth between a first drive position, shown in FIG. 8, and a second drive position, shown in FIG. 9. In order to prevent staple firing before tissue clamping has occurred, the upper latch arm 118 on the release button 30 is engaged with the second notch 148 on the drive member 138 such that the metal drive rod 140 is locked in its proximal-most position, as depicted in FIG. 6. When the upper latch arm 118 falls into the recess 122, the upper latch arm 118 disengages with the second notch 148 to permit distal movement of the metal drive rod 140, as depicted in FIG. 9.

[0067] Because the first gear rack 141 on the drive member 138 and the gear rack 154 on the metal drive rod 140 are engaged with the multiplier 136, movement of the firing trigger 28 causes the metal drive rod 140 to reciprocate between a first reciprocating position, shown in FIG. 8, and a second reciprocating position, shown in FIG. 9. Since the diameter of the first pinion gear 150 is greater than the diameter of the second pinion gear 152, the multiplier 136 moves the reciprocating section 134 a greater distance than the drive member 138 is moved by the firing trigger 28. The diameters of the first and second pinion gears 150 and 152 may be changed to permit the length of the stroke of the firing trigger 28 and the force required to move it to be varied.

[0068] It will be appreciated that the handle portion 20 is illustrative and that other actuation mechanisms may be employed. For instance, the closing and firing motions may be generated by automated means.

SEPARATE AND DISTINCT CLOSING AND FIRING END EFFECTOR

[0069] The end effector 12 of the surgical stapling and severing instrument 10 is depicted in further detail in FIGS. 10-16. As described above, the handle portion 20 produces separate and distinct closing and firing motions that actuate the end effector 12. The end effector 12 advantageously maintains the clinical flexibility of this separate and distinct closing and firing (i.e., stapling and severing). In addition, the end effector 12 introduces the aforementioned ability to affirmatively maintain the closed spacing during firing after the clinician positions and clamps the tissue. Both features procedurally and structurally enhance the ability of the surgical stapling and severing instrument 10 by ensuring adequate spacing for instances where an otherwise inadequate amount of tissue is clamped and to enhance the clamping in in-

stances where an otherwise excessive amount of tissue has been clamped.

[0070] FIG. 10 depicts the end effector 12, which is in an open position by a retracted closure sleeve 32, with a staple cartridge 37 installed in the elongate channel 16. On a lower surface 200 of the anvil 18, a plurality of stapling forming pockets 202 are arrayed to correspond to a plurality of stapler apertures 204 in an upper surface 206 of the staple cartridge 37. The firing bar 14 is at its proximal position, with the upper pin 38 aligned in a non-interfering fashion with the anvil pocket 40. The anvil pocket 40 is shown as communicating with the longitudinal anvil slot 42 in the anvil 18. The distally presented cutting edge 48 of the firing bar 14 is aligned with and proximally from removed from the vertical slot 49 in the staple cartridge 37, thereby allowing removal of a spent cartridge and insertion of an unfired cartridge, which is snapfit into the elongate channel 16. Specifically, extension features 208, 210 of the staple cartridge 37 engage recesses 212, 214 (shown in FIG. 12) of the elongate channel 16.

[0071] FIG. 11 shows the implement portion 22 of the surgical stapling and severing instrument 10 in disassembled form. The staple cartridge 37 is shown as being comprised of a cartridge body 216, a wedge sled 218, single and double drivers 220, staples 222, and a cartridge tray 224. When assembled, the cartridge tray 224 holds the wedge sled 218, single and double drivers 220, and staples 222 inside the cartridge body 216.

[0072] Having a wedge sled 218 integral to the staple cartridge 37 enables a number of flexible design options as compared to incorporating camming surfaces onto a firing bar itself. For instance, a number of different staple cartridges may be selected for use in the instrument 10 with each staple cartridge having a different configuration of rows of staples, each thus having a unique wedge sled configured to contact the middle pin 46 of the firing bar 14 while causing the driving of the staples 222. As another example, the integral wedge sled 218 provides an opportunity for a number of lockout features, described in greater detail in the first and third aforementioned co-pending applications.

[0073] The elongate channel 16 has a proximally placed attachment cavity 226 that receives a channel anchoring member 228 on the distal end of the frame 34 for attaching the end effector 12 to the handle portion 20. The elongate channel 16 also has an anvil cam slot 230 that pivotally receives an anvil pivot 232 of the anvil 18. The closure sleeve 32 that encompasses the frame 34 includes a distally presented tab 234 that engages an anvil feature 236 proximate but distal to the anvil pivot 232 on the anvil 18 to thereby effect opening and closing of the anvil 18. The firing drive member 36 is shown as being assembled from the firing bar 14 attached to a firing connector 238 by pins 240, which in turn is rotatably and proximally attached to the metal drive rod 140. The firing bar 14 is guided at a distal end of the frame by a slotted guide 239 inserted therein.

[0074] With particular reference to FIG. 12, a portion of the staple cartridge 37 is removed to expose portions of the elongate channel 16, such as recesses 212, 214 and to expose some components of the staple cartridge 37 in their unfired position. In particular, the cartridge body 216 (shown in FIG. 11) has been removed. The wedge sled 218 is shown at its proximal, unfired position with a pusher block 242 contacting the middle pin 46 (not shown in FIG. 12) of the firing bar 14. The wedge sled 218 is in longitudinal sliding contact upon the cartridge tray 224 and includes wedges 228 that force upward the single and double drivers 220 as the wedge sled 218 moves distally. Staples 222 (not shown in FIG. 12) resting upon the drivers 220 are thus also forced upward into contact with the anvil forming pockets 202 on the anvil 18 to form closed staples. Also depicted is the channel slot 45 in the elongate channel 16 that is aligned with the vertical slot 49 in the staple cartridge 37.

[0075] FIG. 13 depicts the end effector 12 of FIG. 12 with all of the staple cartridge 37 removed to show the middle pin 46 of the firing bar 14 as well as portion of the elongate channel 16 removed adjacent to the channel slot 45 to expose the firing bar cap 44. In addition, portions of the shaft 23 are removed to expose a proximal portion of the firing bar 14. Projecting downward from the anvil 18 near the pivot, a pair of opposing tissue stops 244 prevent tissue being positioned too far up into the end effector 12 during clamping.

[0076] FIG. 14 depicts the end effector 12 closed in a tissue clamping position with the firing bar 14 unfired. The upper pin 38 is in the anvil pocket 40, vertically aligned with the anvil slot 42 for distal longitudinal movement of the firing bar 14 during firing. The middle pin 46 is positioned to push the wedge sled 218 distally so that wedge 228 sequentially contacts and lifts double drivers 220 and the respective staples 222 into forming contact with staple forming pockets 202 in the lower surface 200 of the anvil 18.

[0077] FIG. 15 depicts the upper surface 206 of the staple cartridge 37 with the firing bar 14 in its unfired, proximal position. The stapler apertures 204 are arrayed on each side of the vertical slot 49 in the staple cartridge 37.

[0078] FIG. 16 depicts the end effector 12 near the pivot showing that the elongate channel 16 has opposing ramp portions 246 to thereby cooperate with the tissue stops 244 of the anvil 18 (not shown in FIG. 16) to prevent tissue from jamming the end effector 12. Also depicted in greater detail are the double drivers 220 and their relation to the staples 222.

OPERATION

[0079] In use, the surgical stapling and severing instrument 10 is used as depicted in FIGS 1, 2, and 17-23. In FIGS. 1-2, the instrument 10 is in its start position, having had an unfired, fully loaded staple cartridge 37 snap-fitted into the distal end of the elongate channel 16. Both trig-

gers 26, 28 are forward and the end effector 12 is open, such as would be typical after inserting the end effector 12 through a trocar or other opening into a body cavity. The instrument 10 is then manipulated by the clinician such that tissue 248 to be stapled and severed is positioned between the staple cartridge 37 and the anvil 18, as depicted in FIG. 17.

[0080] With reference to FIGS. 18-19, next, the clinician moves the closure trigger 26 proximally until positioned directly adjacent to the pistol grip 24, locking the handle portion 20 into the closed and clamped position. The retracted firing bar 14 in the end effector 12 does not impede the selective opening and closing of the end effector 12, but rather resides within the anvil pocket 40. With the anvil 18 closed and clamped, the E-beam firing bar 14 is aligned for firing through the end effector 12. In particular, the upper pin 38 is aligned with the anvil slot 42 and the elongate channel 16 is affirmatively engaged about the channel slot 45 by the middle pin 46 and the firing bar cap 44.

[0081] With reference to FIGS. 20-21, after tissue clamping has occurred, the clinician moves the firing trigger 28 proximally causing the firing bar 14 to move distally into the end effector 12. In particular, the middle pin 46 enters the staple cartridge 37 through the firing drive slot 47 to effect the firing of the staples 222 (not shown in FIGS. 20-21) via wedge sled 218 toward the anvil 18. The lower most pin, or firing bar cap 44, cooperates with the middle pin 46 to slidably position cutting edge 48 of the firing bar 14 to sever tissue. The two pins 44, 46 also position the upper pin 38 of the firing bar 14 within longitudinal anvil slot 42 of the anvil 18, affirmatively maintaining the spacing between the anvil 18 and the elongate channel 16 throughout its distal firing movement.

[0082] With reference to FIGS. 22-23, the clinician continues moving the firing trigger 28 until brought proximal to the closure trigger 26 and pistol grip 24. Thereby, all of the ends of the staples 222 are bent over as a result of their engagement with the anvil 18. The firing bar cap 44 is arrested against a firing bar stop 250 projecting toward the distal end of the channel slot 45. The cutting edge 48 has traversed completely through the tissue. The process is complete by releasing the firing trigger 28 and by then depressing the release button 30 while simultaneously squeezing the closure trigger 26 to open the end effector 12.

[0083] While the present invention has been illustrated by description of several embodiments and while the illustrative embodiments have been described in considerable detail, it is not the intention of the applicant to restrict or in any way limit the scope of the appended claims to such detail. Additional advantages and modifications may readily appear to those skilled in the art.

[0084] For example, the affirmative spacing of the anvil 18 and elongate channel 16 is achieved in part with two pins 44, 46 on the firing bar 14 engaging opposite sides of a channel slot 47 and a single upper pin 38 entrained within an anvil slot 42. It would be consistent with aspects

of the invention for the anvil to be captured by opposing pins on either side of a longitudinal slot and/or for an elongate channel to have an internal slot that entrains a lower pin.

[0085] For another example, although the E-beam firing beam 14 has advantages for an endoscopically employed surgical severing and stapling instrument 10, a similar E-Beam may be used in other clinical procedures. It is generally accepted that endoscopic procedures are more common than laparoscopic procedures. Accordingly, the present invention has been discussed in terms of endoscopic procedures and apparatus. However, use herein of terms such as "endoscopic", should not be construed to limit the present invention to a surgical stapling and severing instrument for use only in conjunction with an endoscopic tube (i.e., trocar). On the contrary, it is believed that the present invention may find use in any procedure where access is limited to a small incision, including but not limited to laparoscopic procedures, as well as open procedures.

[0086] For yet another example, although an illustrative handle portion 20 described herein is manually operated by a clinician, it is consistent with aspects of the invention for some or all of the functions of a handle portion to be powered (e.g., pneumatic, hydraulic, electro-mechanical, ultrasonic, etc.). Furthermore, controls of each of these functions may be manually presented on a handle portion or be remotely controlled (e.g., wireless remote, automated remote console, etc.).

[0087] As yet an additional example, although a simultaneous stapling and severing instrument is advantageously illustrated herein, it would be consistent with aspects of the invention for stapling to comprise other types of fasteners and attachment techniques.

SPENT CARTRIDGE LOCKOUT

[0088] As described above, the E-beam firing bar 14 provides unique capabilities for affirmatively spacing the end effector 12 while simultaneously severing tissue and effecting the forming of staples on each side of the cut. Preventing the distal movement of the firing bar 14 thus prevents the inadvertent severing of tissue. A spent cartridge lockout mechanism 270 advantageously responds to a spent staple cartridge 37 by blocking the middle pin 46 of the firing bar 14 (only the middle pin of the firing bar being shown in FIG. 24).

[0089] In particular, the spent cartridge lockout mechanism 270 is depicted as being incorporated into a cartridge body 272 with blocking members 274 resiliently positioned above the wedge sled 218 (not shown in FIG. 24). In particular, the blocking members 274 each reside within a downward and proximally opening cavity 276. Each block member 274 includes a leaf spring end 277 that is held within the cavity 276.

[0090] The cavities 276 are vertically aligned and spaced and parallel about the vertical slot 49. The cartridge body 272 also includes wedge slots 278 that lon-

gitudinally pass through the cartridge, being open from a portion of a proximal and underside of the cartridge body 272 to receive individual wedges of the wedge sled 218 (not shown in FIG. 24).

[0091] Each lockout mechanism 270 has a deflectable end 280 shaped to reside within the respective cavity 276 when depressed and to impede a distally moving middle pin 46 of a firing bar 14 when released.

[0092] FIGS. 25-28 depict the lockout mechanism 270 sequentially as the surgical stapling and severing instrument 10 is fired. In Fig. 25, an unfired staple cartridge 37 has been inserted into the elongate channel 16 with the wedge sled 218 depressing upward the deflectable ends 280 so that the firing drive slot 47 formed between the cartridge body 216 and the cartridge tray 224 is unimpeded.

[0093] In FIG. 26, firing of the cartridge 37 has commenced with the wedge sled 218 and the middle pin 46 of the firing bar 14 having distally traversed past the deflectable ends 280, which then spring down into the firing drive slot 47.

[0094] In FIG. 27, the staple cartridge 37 is now spent with the wedge sled 218 fully driven distally and no longer depicted. The firing bar 14 is being retracted proximally. Since the deflectable ends 280 pivot from a more distal point, the firing bar 14 is able to ride under the deflectable ends 280 during retraction, causing them to be depressed up, out of the firing drive slot 47.

[0095] In FIG. 28, the firing bar 14 is fully retracted and now confronts a non-depressed (released) pair of deflectable ends 280 to prevent distal movement. The single lockout mechanism 270 thereby activated remains during the period in which the spent staple cartridge 37 is removed until an unfired staple cartridge 37 is installed.

[0096] FIG. 29 depicts another lockout mechanism 290, depicted as an integral lockout hook 292 formed as part of a cartridge body 294. In particular, a proximally directed wedge shaped recess 296 defines proximally directed shaft 298 that terminates in a downwardly projecting hook end 300. It will be appreciated that the cartridge body 294 is depicted partially cut away showing only one lockout hook 292, although a pair may advantageously be used, one on each side of the vertical slot 49 (not shown in FIG. 29). Thus, the lockout mechanism 290 may be economically incorporated into a staple cartridge 37 without additional assembly steps.

[0097] FIGS. 30-33 depict the sequence of operation of the integral lockout hooks 292. In FIG. 30, the staple cartridge 37 is unfired so that the distally positioned wedge sled 218 depresses upwardly the hook ends 300 into the wedge shaped recess 296, allowing the middle pin 46 of the firing bar 14 to move distally during firing, as depicted in FIG. 31. With the wedge sled 218 and middle pin 46 distally removed with respect to the lockout hooks 292, the lockout hooks 292 resiliently returns to its released position, with hooks end 300 occupying the firing drive slot 47.

[0098] In FIG. 32, the firing bar 14 is being retracted

to the point of contacting the hook ends 300 of the lockout hook 292. Since the distal edge of the hook ends 300 is ramped downward proximally, the middle pin 46 of the firing bar 14 rides under the hook ends 300, forcing them up into the wedge shaped recess 296 until middle pin 46 is past the hook ends 300, as depicted in FIG. 33 wherein the hook ends 300 resiliently spring back down to block the middle pin 46. Thus, the firing bar 14 is prevented from distal movement while the spent staple cartridge 37 remains in the elongate channel 16.

[0099] While the present invention has been illustrated by description of several embodiments and while the illustrative embodiments have been described in considerable detail, it is not the intention of the applicant to restrict or in any way limit the scope of the appended claims to such detail. Additional advantages and modifications may readily appear to those skilled in the art.

[0100] For example, although a lockout mechanism comprised of a pair of fingers or hooks has been depicted, some applications may rely upon only one such structure.

[0101] As another example, although the middle pin 46 of the firing bar is engaged by the locking mechanism, in some applications the locking member may impede the another portion of a firing bar, such as a vertical surface or a lower cap.

[0102] As yet an additional example, although a staple cartridge advantageously allows reuse of most of the end effector, applications of the lockout mechanism may be in disposable end effectors that are replaced after each firing.

Claims

1. A staple cartridge (37) having a proximal and a distal end for use in a surgical instrument (10) having a firing device, said staple cartridge (37) comprising:

a plurality of drivers (200) supporting a plurality of staples (222);
 an initially proximally positioned wedge sled (218) adapted to be moved to and left in a distal position by firing a said firing device;
 a body (216, 272) having a longitudinal wedge cavity (278) that communicates transversely with a plurality of staple apertures (204), said wedge cavity (278) open proximally to receive said wedge sled (218);
 said plurality of staples (222) positioned in said staple apertures (204);
 said plurality of drivers (220) supporting said staples (222) sized to translate from said wedge cavity (278) into said staple apertures (204);
 a cartridge tray (224);
 a firing drive slot (47) formed between said cartridge body (216, 272) and said cartridge tray (224), said firing drive slot (47) being traversable by a said firing device; and

a lockout device (270, 290) comprising a movable blocking member (274, 292) coupled with and incorporated with in said cartridge body (216, 272) and movable between position in a lockout recess (296) defined in said cartridge body (216, 272) and a position occupying a proximal portion of said firing drive slot (47) traversed by a said firing device; wherein said wedge sled (218), when proximally positioned in said wedge cavity (278) in an unfired position thereof, depresses a deflectable end (280, 300) of said movable member (274, 292) into said recess (296), such that a said firing device is not impeded from moving distally therethrough; and wherein; after firing of a said firing device, and said wedge sled (218) having distally traversed past said deflectable end (280) of said movable blocking member (274, 292), said deflectable end (280) is thereby released into the firing drive slot (47) to block subsequent distal movement of a said firing device from a fully retracted position of a said firing device.

2. The staple cartridge (37) of claim 1, wherein said deflectable end (280, 300) of said movable blocking member (274, 292) has a ramped distal side and a blocking proximal side.
3. The staple cartridge (37) of claim 2, wherein said cartridge body (216, 272) comprises a resilient material, said lockout device (270, 290) comprises a proximally projecting finger with a projecting hook end (300) formed integrally with said body (216, 272).
4. The staple cartridge (37) of claim 2, wherein said movable blocking member (274, 290) of said lockout device (270, 290) is springedly attached to said cartridge body (216, 272).
5. A surgical instrument (10), comprising:
 - a handle means (20) for producing a closing motion and a firing motion;
 - an implement means for clamping upon tissue in response to the closing motion and for severing clamped tissue in response to the firing motion; and
 - a stapling means responsive to the firing means to staple the severed tissue and responsive to a spent stapling condition to prevent firing;
 said surgical instrument (10), comprising:
 - a pair of pivotally opposing jaws;
 - a firing device positioned for longitudinal movement between said opposing jaws;
 - a handle portion (20) operably configured

to close the opposing jaws and to fire the firing device;
a staple cartridge (37) according to any previous claim 1-4, engageable in said opposing jaws.

6. The surgical instrument (10) of claim 5, wherein said firing device comprises a firing bar (14) having a vertical cutting edge (48), the cartridge body (216, 272) including a proximally opening vertical slot (49) registered to receive said vertical cutting edge (48).
7. The surgical instrument (10) of claim 6, wherein said firing bar (14) includes a pin (46) projecting transverse to said cutting edge (48) for sliding engagement to said firing drive slot (47), registered to receive said pin (46), said lockout device (270, 290) comprising a pair of movable blocking members (274, 276) positioned offset laterally from the vertical slot (49) and for engaging the pin (46).

Patentansprüche

1. Klammerpatrone (37), die ein proximales Ende und ein distales Ende aufweist, zur Nutzung in einem chirurgischen Gerät (10), das eine Schussvorrichtung aufweist, umfassend:
 - mehrere Antriebe (220), die mehrere Klammern (222) halten;
 - einen anfangs proximal positionierten Keilschlitten (218), der durch Auslösen der Schussvorrichtung zum Bewegen in eine distale Position und zum Verbleiben in einer distalen Position ausgelegt ist;
 - einen Körper (216, 272), der einen longitudinalen Keilhohlraum (278) aufweist, der mit mehreren Klammeröffnungen (204) in Querrichtung verbunden ist, wobei sich der Keilhohlraum (278) proximal öffnet, um den Keilschlitten (218) aufzunehmen;
 - mehrere Klammern (222), die in den Klammeröffnungen (204) positioniert sind; mehrere Antriebe (220), die die Klammern (222) halten, welche für eine Verlagerung von dem Keilhohlraum (278) in die Klammeröffnungen (204) bemessen sind; eine Patronenablage (224);
 - einen Schussantriebsschlitz (47), der zwischen dem Patronenkörper (216, 272) und der Patronenablage (224) ausgebildet ist, wobei der Schussantriebsschlitz (47) von der Schussvorrichtung durchquerbar ist; und
 - eine Sperre (270, 290), die ein bewegliches Sperrbauteil (274, 292) umfasst, das mit dem Patronenkörper (216, 272) gekoppelt ist und innerhalb des Patronenkörpers (216, 272) integriert ist und beweglich zwischen einer Position

- in einer Sperraussparung (296), die in dem Patronenkörper (216, 272) definiert ist, und einer Position angeordnet ist, die einen proximalen Abschnitt des Schussantriebsschlitzes (47) belegt, welcher durch die Schussvorrichtung durchquert wird; wobei
- der Keilschlitten (218), wenn er sich proximal in dem Keilhohlraum (278) in einer nicht geschossenen Position befindet, ein ablenkbares Ende (280, 300) des beweglichen Bauteils (274, 292) in die Aussparung (296) drückt, so dass die Schussvorrichtung nicht daran gehindert wird, sich **dadurch** distal zu bewegen; und wobei,
- nachdem die Schussvorrichtung ausgelöst wurde und sich der Keilschlitten (218) distal an dem ablenkbaren Ende (280) der beweglichen Sperrbauteile (274, 292) vorbei querverlagert hat, das ablenkbare Ende (280) **dadurch** in den Schussantriebsschlitz (47) freigegeben ist, um eine nachfolgende distale Bewegung der Schussvorrichtung von einer vollständig zurückgezogenen Position der Schussvorrichtung zu sperren.
2. Klammerpatrone (37) nach Anspruch 1, wobei das ablenkbare Ende (280, 300) des beweglichen Sperrbauteils (274, 292) eine rampenartige distale Seite und eine sperrende proximale Seite aufweist.
3. Klammerpatrone (37) nach Anspruch 2, wobei der Patronenkörper (216, 272) ein elastisches Material umfasst, wobei die Sperre (270, 290) einen proximalen vorstehenden Finger mit einem vorstehenden Hakenende (300) umfasst, das mit dem Körper (216, 272) integriert geformt ist.
4. Klammerpatrone (37) nach Anspruch 2, wobei das bewegliche Sperrbauteil (274, 292) der Sperre (270, 290) federnd an dem Patronenkörper (216, 272) angebracht ist.
5. Chirurgisches Gerät (10) umfassend:
- einen Griff (20) zum Erzeugen einer Schließbewegung und einer Schussbewegung; eine Einrichtung zum Klemmen von Gewebe als Reaktion auf die Schließbewegung und zum Trennen von geklammerten Gewebe als Reaktion auf die Schussbewegung; und
- einen Klammerer, das auf das Auslösen der Schussvorrichtung anspricht, um das abgetrennte Gewebe zu klammern, und das auf einen verbrauchten Klammerzustand anspricht, um das Schießen zu verhindern;
- ein Paar sich schwenkbar gegenüberliegende Backen;
- eine Schussvorrichtung, die für eine Längsbewegung zwischen den sich gegenüberliegenden

den Backen positioniert ist;

einen Griffabschnitt (20), der betriebsgemäß zum Schließen der sich gegenüberliegenden Backen und zum Auslösen der Schussvorrichtung konfiguriert ist;

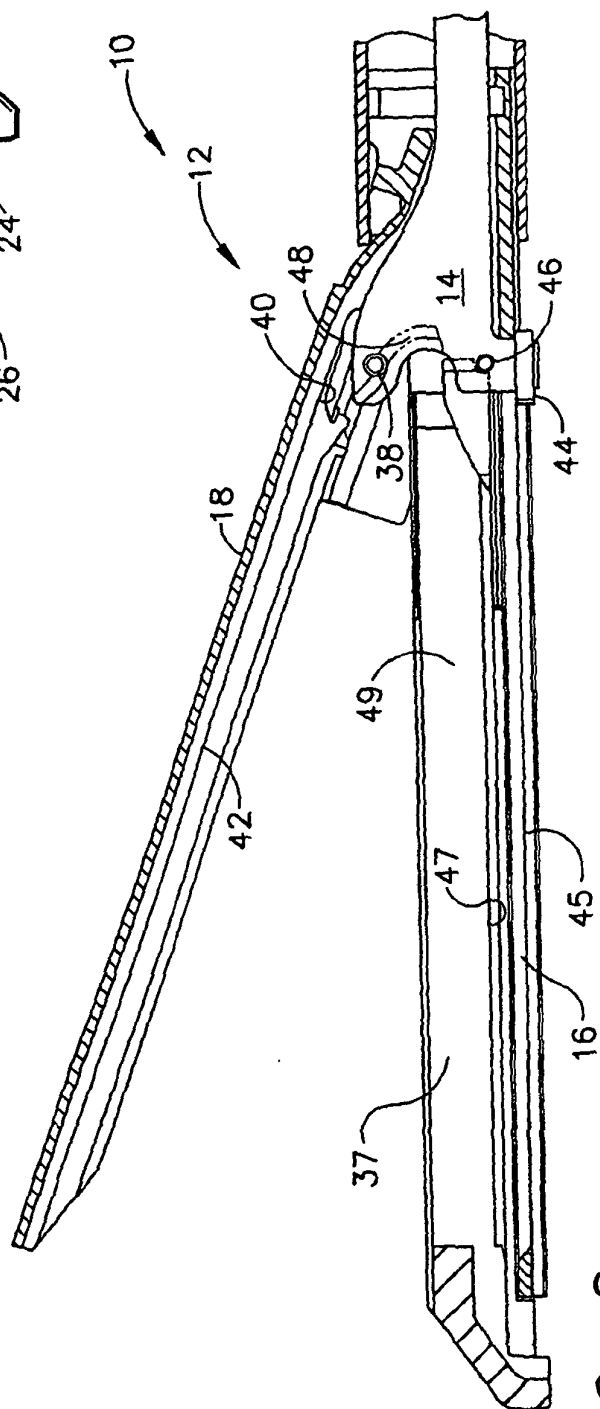
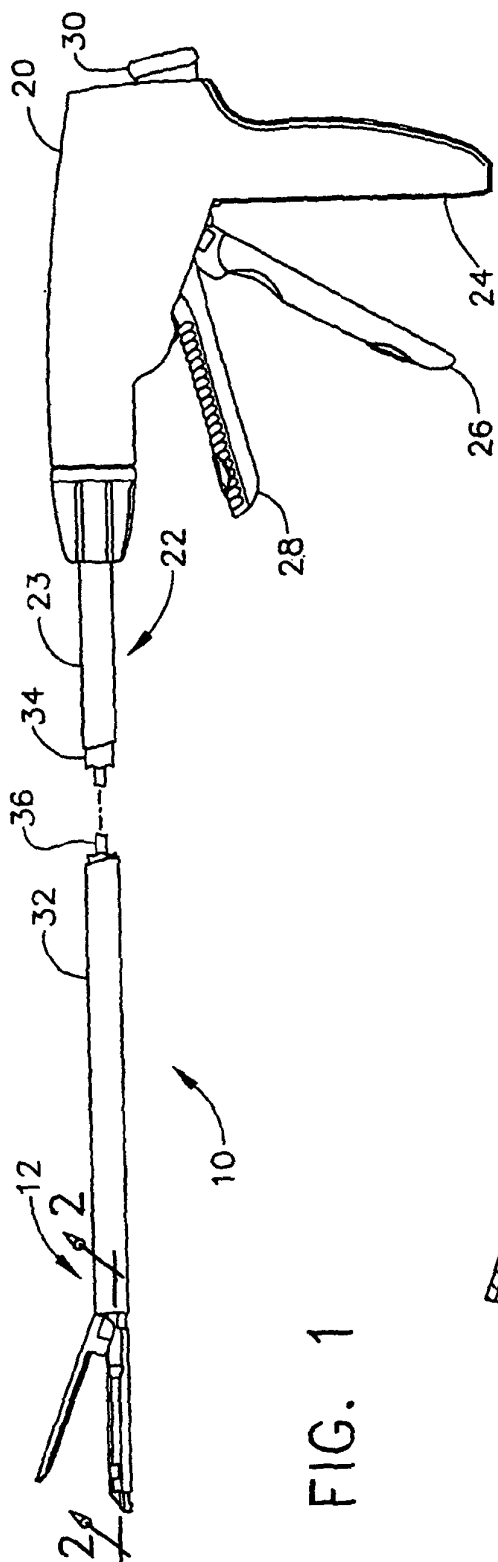
eine nach einem der Ansprüche 1 bis 4 ausgebildete Klammerpatrone (37), die mit den gegenüberliegenden Backen in Eingriff kommen kann.

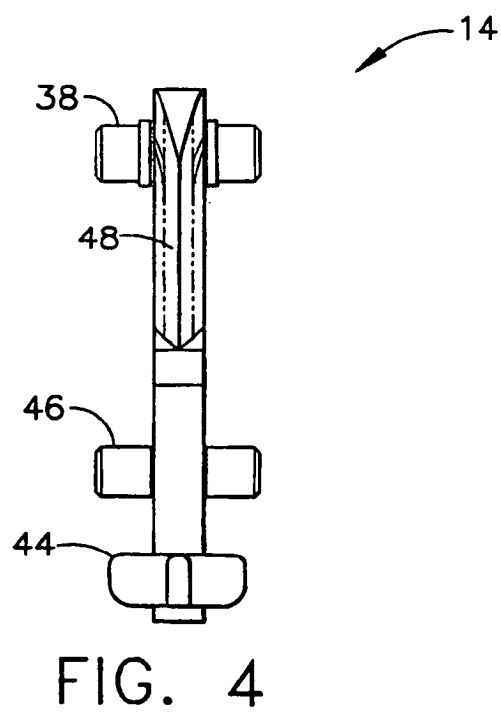
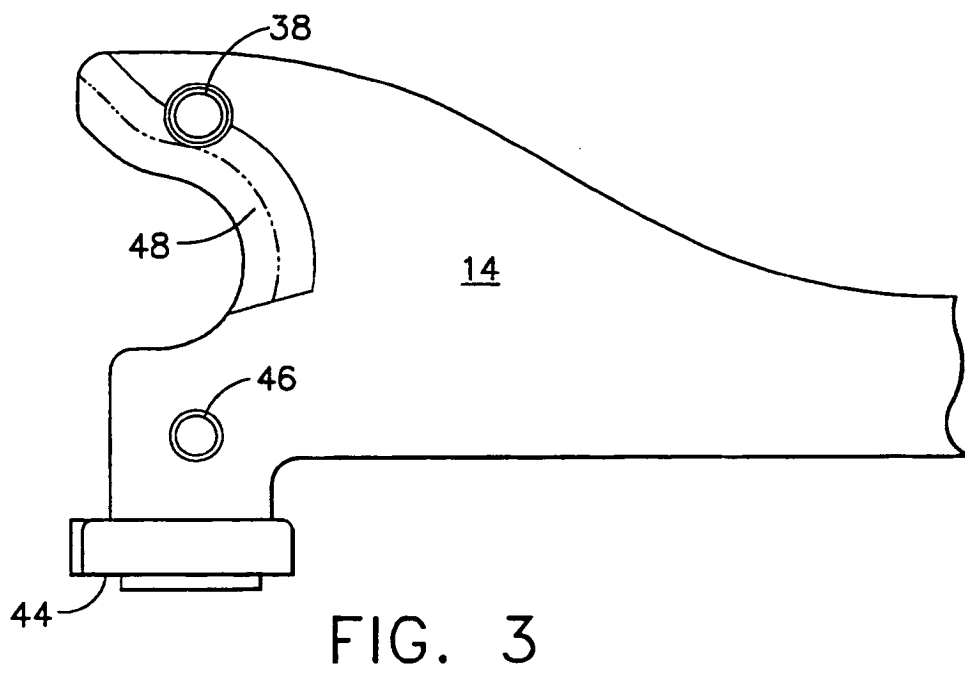
6. Chirurgisches Gerät (10) nach Anspruch 5, wobei die Schussvorrichtung eine Schussstange (14) umfasst, die eine vertikale Schneide (48) aufweist, wobei der Patronenkörper (216, 272) einen proximal offenen vertikalen Schlitz (49) aufweist, der die Aufnahme der vertikalen Schneide (48) zulässt.
7. Chirurgisches Gerät (10) nach Anspruch 6, wobei die Schussstange (14) einen Stift (46) umfasst, der in Querrichtung zur Schneide (48) vorsteht, um den Eingriff zu dem Schussantriebsschlitz (47) zu schieben, der die Aufnahme des Stiftes (46) zulässt, wobei die Sperrvorrichtung (270, 290) ein Paar bewegliche Sperrbauteile (274, 276) umfasst, das lateral versetzt von dem vertikalen Schlitz (49) und zum Eingriff mit dem Stift (46) positioniert ist.

Revendications

1. Cartouche d'agrafes (37) comprenant une extrémité distale et une extrémité proximale destinée à être utilisée dans un instrument chirurgical (10) comportant un dispositif de percussion, ladite cartouche d'agrafes (37) comprenant :
- ♦ une pluralité de guides (200) supportant une pluralité d'agrafes (222) ;
 - ♦ une coulisse en V positionnée initialement de façon proximale (218) adaptée pour être déplacée vers, et laissée, dans une position distale par percussion dudit dispositif de percussion ;
 - ♦ un corps (216, 272) doté d'une cavité longitudinale en V (278) qui communique dans le sens transversal avec une pluralité d'ouvertures pour agrafes (204), ladite cavité en V (278) étant ouverte de façon proximale pour recevoir ladite coulisse en V (218);
 - ♦ ladite pluralité d'agrafes (222) étant positionnées dans lesdites ouvertures pour agrafes (204) ;
 - ♦ ladite pluralité de guides (220) supportant lesdites agrafes (222) étant dimensionnés pour effectuer une translation depuis ladite cavité en V (278) vers lesdites ouvertures pour agrafes (204) ;
 - ♦ un bac à cartouches (224);
 - ♦ une fente de guidage de percussion (47) for-

- mée entre ledit corps de cartouche (216, 272) et ledit bac à cartouches (224), ladite fente de guidage de percussion (47) pouvant être traversée par un dit dispositif de percussion ; et
- ♦ un dispositif de verrouillage (270, 290) composé d'un élément de blocage mobile (274, 292) accouplé à, et incorporé dans, ledit corps de cartouche (216, 272) et déplaçable entre une position située dans un renforcement de verrouillage (296) défini dans ledit corps de cartouche (216, 272) et une position occupant une partie proximale de ladite fente de guidage de percussion (47) traversée par un dit dispositif de percussion ; dans lequel
 - ♦ ladite coulisse en V (218), lorsqu'elle est positionnée de façon proximale dans ladite cavité en V (278), dans une position non percutée de celle-ci, presse une extrémité flexible (280, 300) dudit élément de blocage mobile (274, 292) vers ledit renforcement (296), de façon à ce qu'un dit dispositif de percussion ne soit pas empêché de se déplacer à travers celle-ci de manière distale; et dans lequel :
 - ♦ après percussion dudit dispositif de percussion, et ladite coulisse en V (218) ayant traversé de manière distale au-delà de ladite extrémité flexible (280) dudit élément de blocage mobile (274, 292), ladite extrémité flexible (280) est ainsi libérée vers la fente de guidage de percussion (47) afin de bloquer un déplacement distal ultérieur d'un dit dispositif de percussion à partir d'une position entièrement rétractée d'un dit dispositif de percussion.
2. Cartouche d'agrafes (37) selon la revendication 1, dans laquelle ladite extrémité flexible (280, 300) dudit élément de blocage mobile (274, 292) présente un côté distal incliné et un côté proximal de blocage.
 3. Cartouche d'agrafes (37) selon la revendication 2, dans laquelle ledit corps de cartouche (216, 272) est composé d'un matériau élastique, ledit dispositif de verrouillage (270, 290) étant composé d'un doigt saillant de façon proximale, avec une extrémité de crochet saillante (300) formée d'une seule pièce avec ledit corps (216, 272).
 4. Cartouche d'agrafes (37) selon la revendication 2, dans laquelle ledit élément de blocage mobile (274, 290) dudit dispositif de verrouillage (270, 290) est fixé par un ressort audit corps de cartouche (216, 272).
 5. Instrument chirurgical (10), comprenant :
 - ♦ un moyen formant poignée (20) destiné à pro-
- duire un mouvement de fermeture et un mouvement de percussion ;
- ♦ un moyen du type outil pour enserrer le tissu en réponse au mouvement de fermeture et pour disjoindre le tissu enserré en réponse au mouvement de percussion ; et
 - ♦ un moyen d'agrafage réagissant au moyen de percussion pouragrafer le tissu disjoint, et réagissant à un état d'agrafe utilisée afin d'empêcher une percussion ;
 - ♦ ledit instrument chirurgical (10) comprenant:
 - ♦ une paire de mâchoires se faisant face par pivotement ;
 - ♦ un dispositif de percussion positionné pour un déplacement longitudinal entre lesdites mâchoires se faisant face;
 - ♦ une partie formant poignée (20) configurée pour fonctionner par fermeture des mâchoires se faisant face et par déclenchement du dispositif de percussion ;
 - ♦ une cartouche d'agrafes (37) selon l'une quelconque des revendications précédentes 1 à 4, insérable dans lesdites mâchoires se faisant face.
6. Instrument chirurgical (10) selon la revendication 5, dans lequel ledit dispositif de percussion comprend une barre de percussion (14) ayant un bord tranchant vertical (48), le corps de cartouche (216, 272) comprenant une fente verticale s'ouvrant de façon proximale (49), adaptée pour recevoir ledit bord tranchant vertical (48).
 7. Instrument chirurgical (10) selon la revendication 6, dans lequel ladite barre de percussion (14) comprend une goupille (46) s'étendant dans le sens transversal vers ledit bord tranchant (48) pour s'insérer en coulissant dans ladite fente de guidage de percussion (47) adaptée pour recevoir ladite goupille (46), ledit dispositif de verrouillage (270, 290) étant composé d'une paire d'éléments de blocage mobiles (274, 276) positionnés en étant décalés latéralement par rapport à la fente verticale (49) et destinés à venir en prise avec la goupille (46).





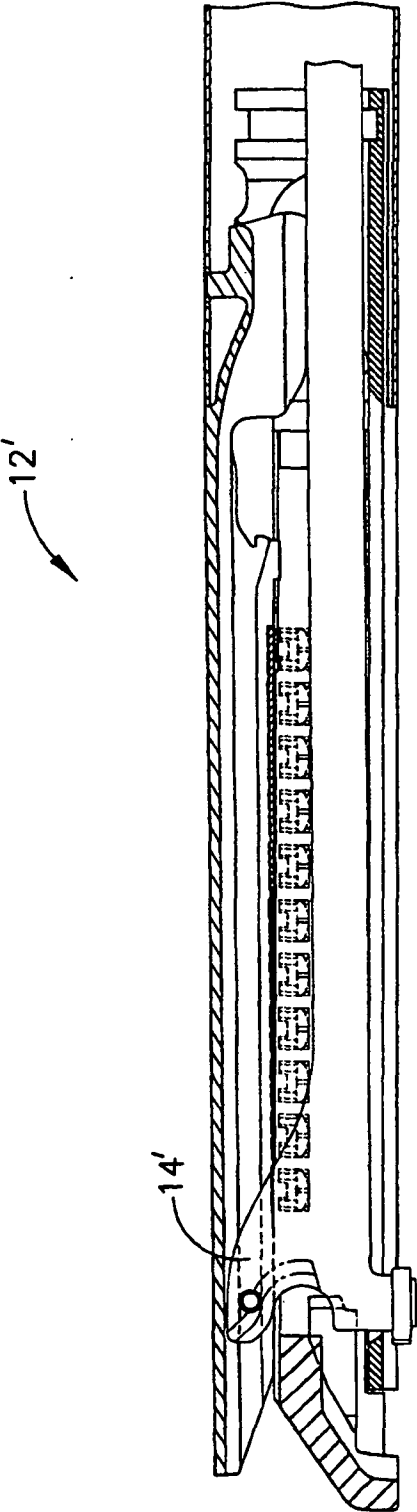


FIG. 5

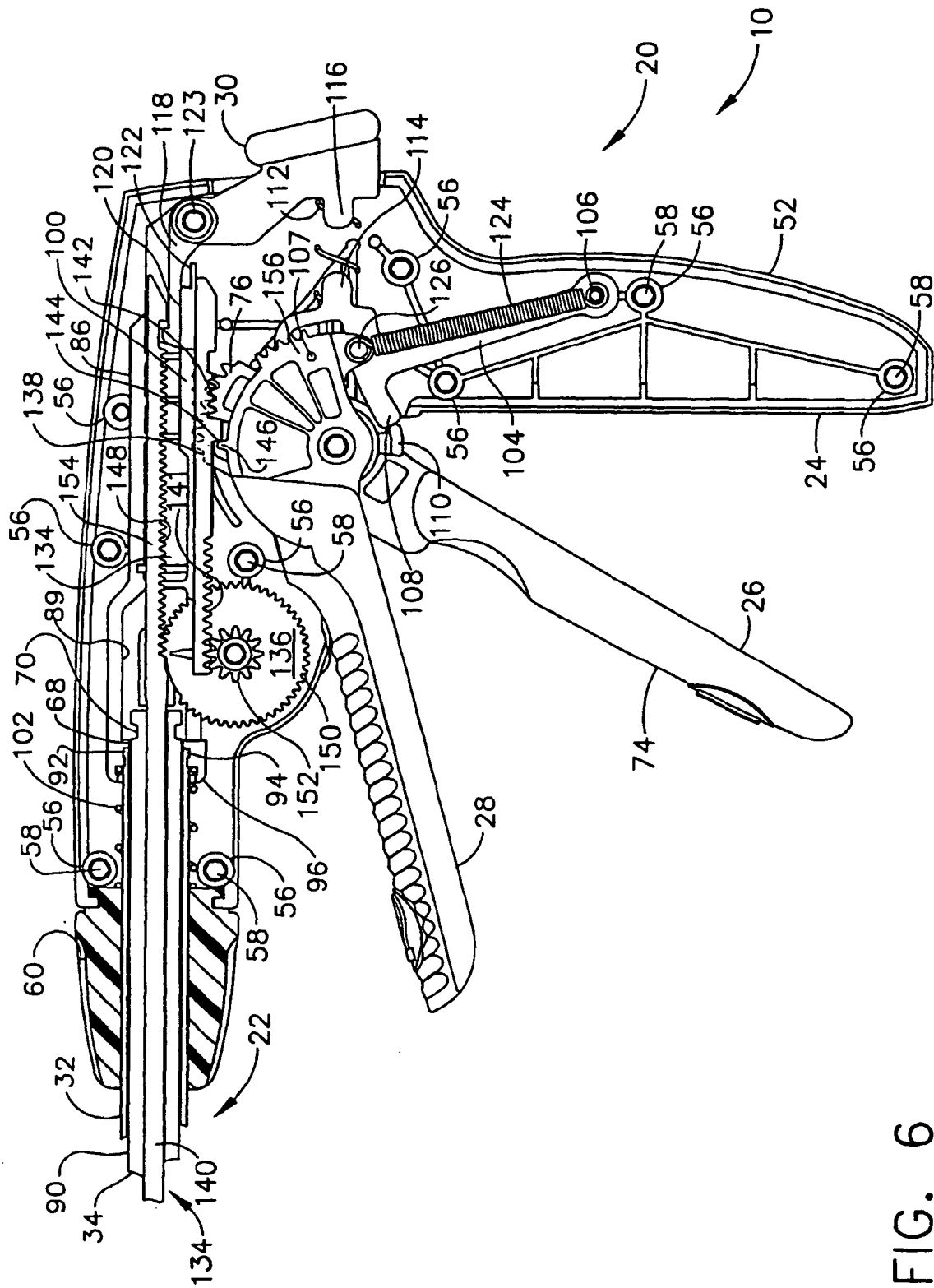


FIG. 6

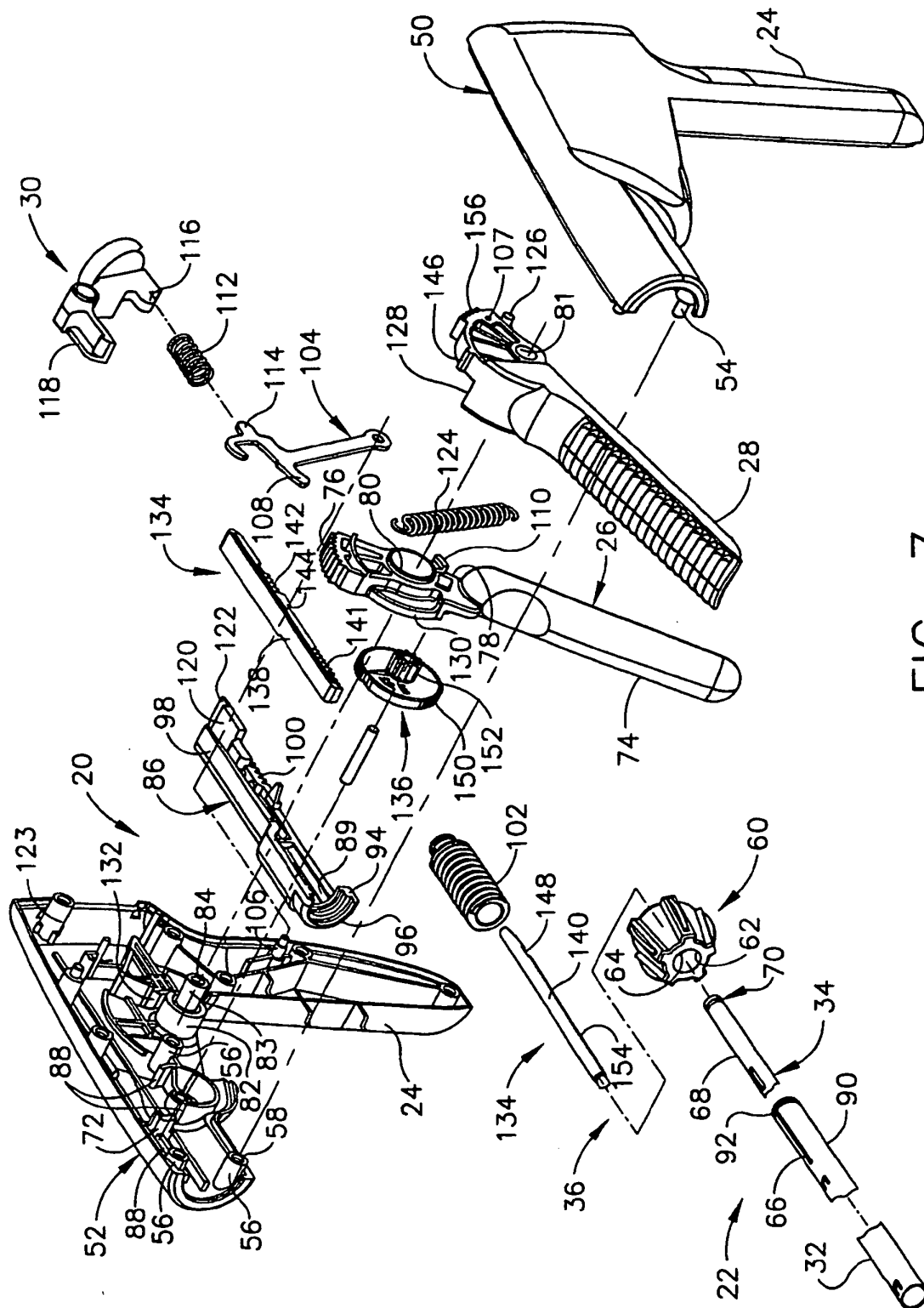


FIG. 7

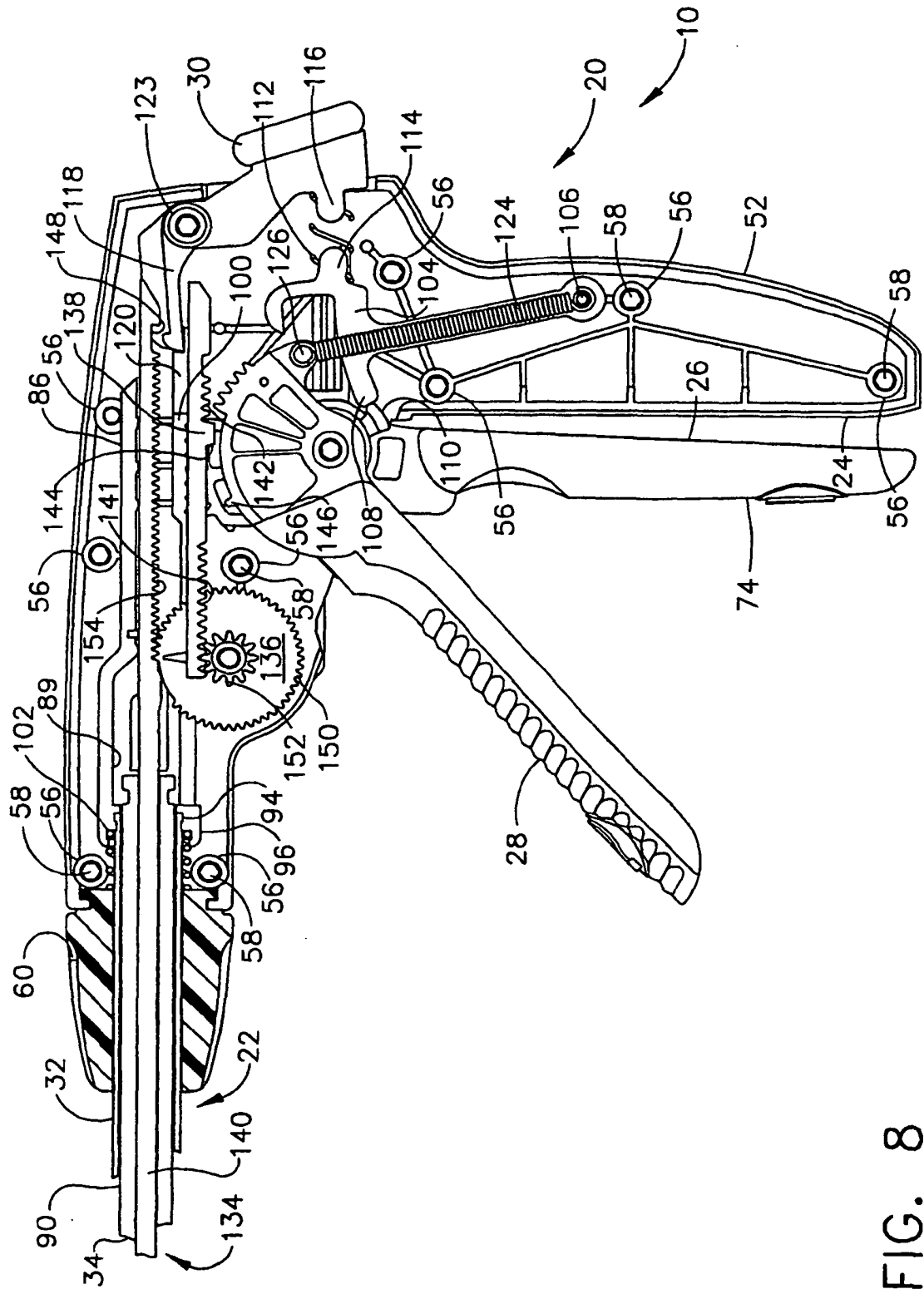
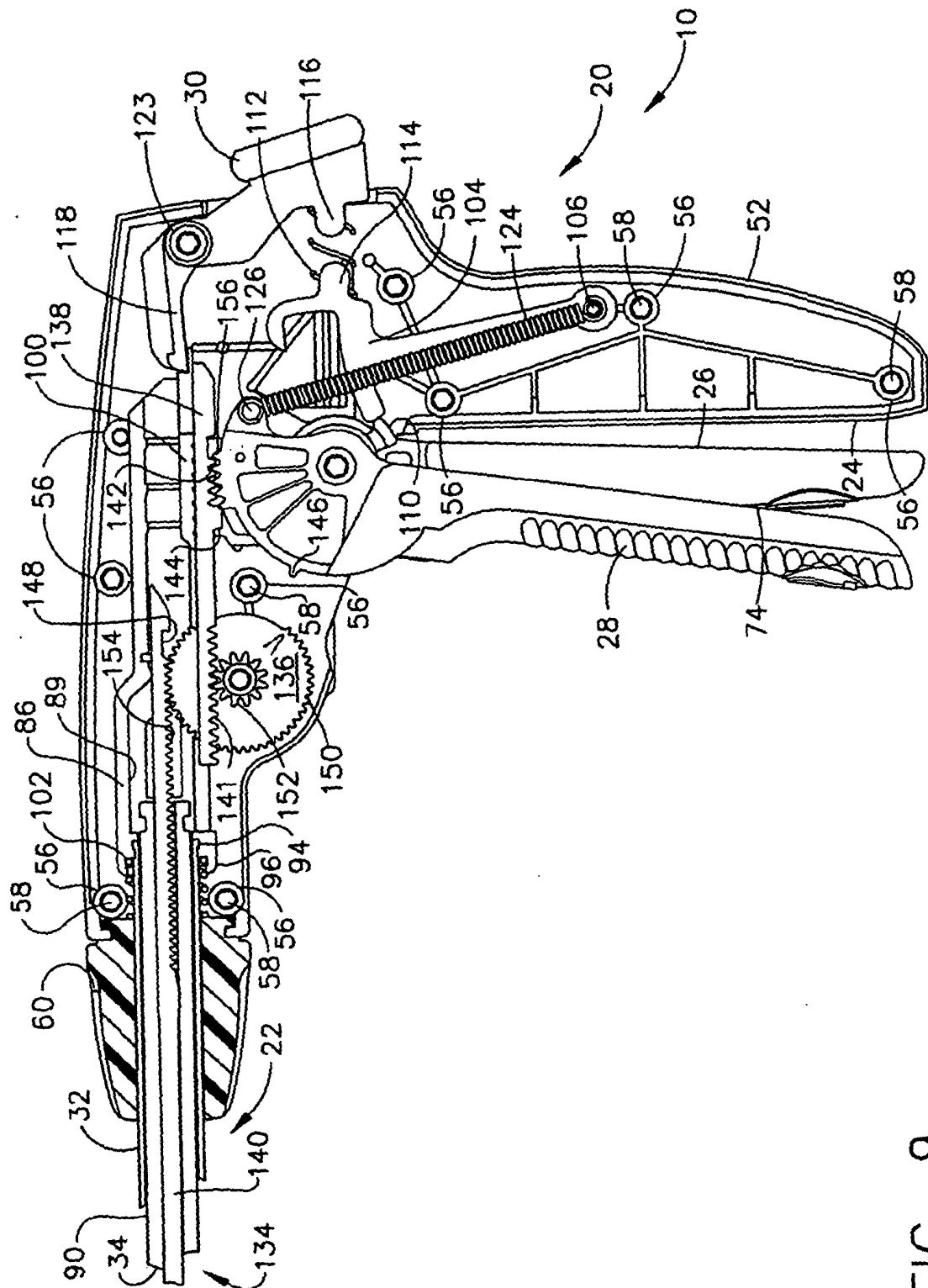


FIG. 8



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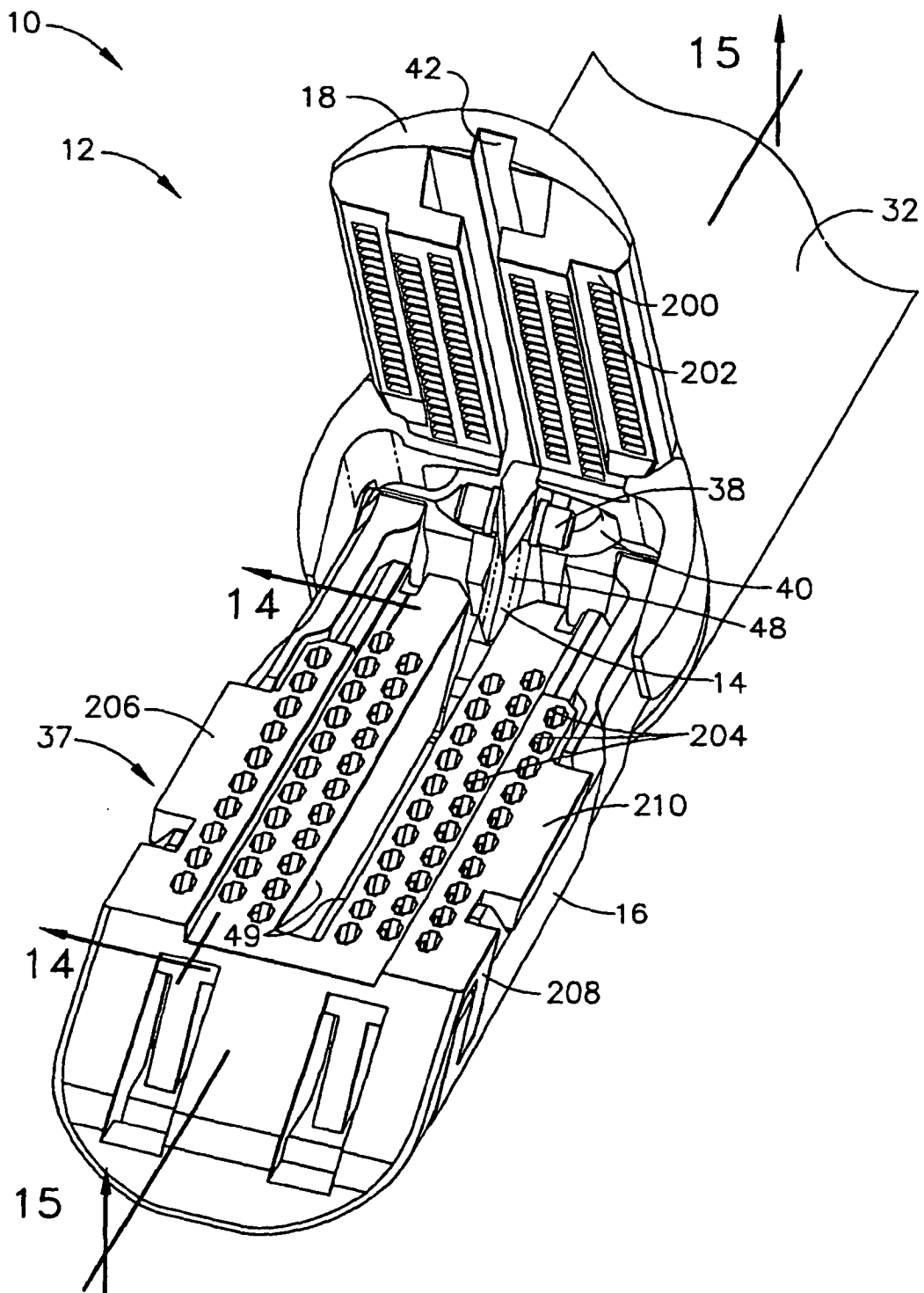


FIG. 10

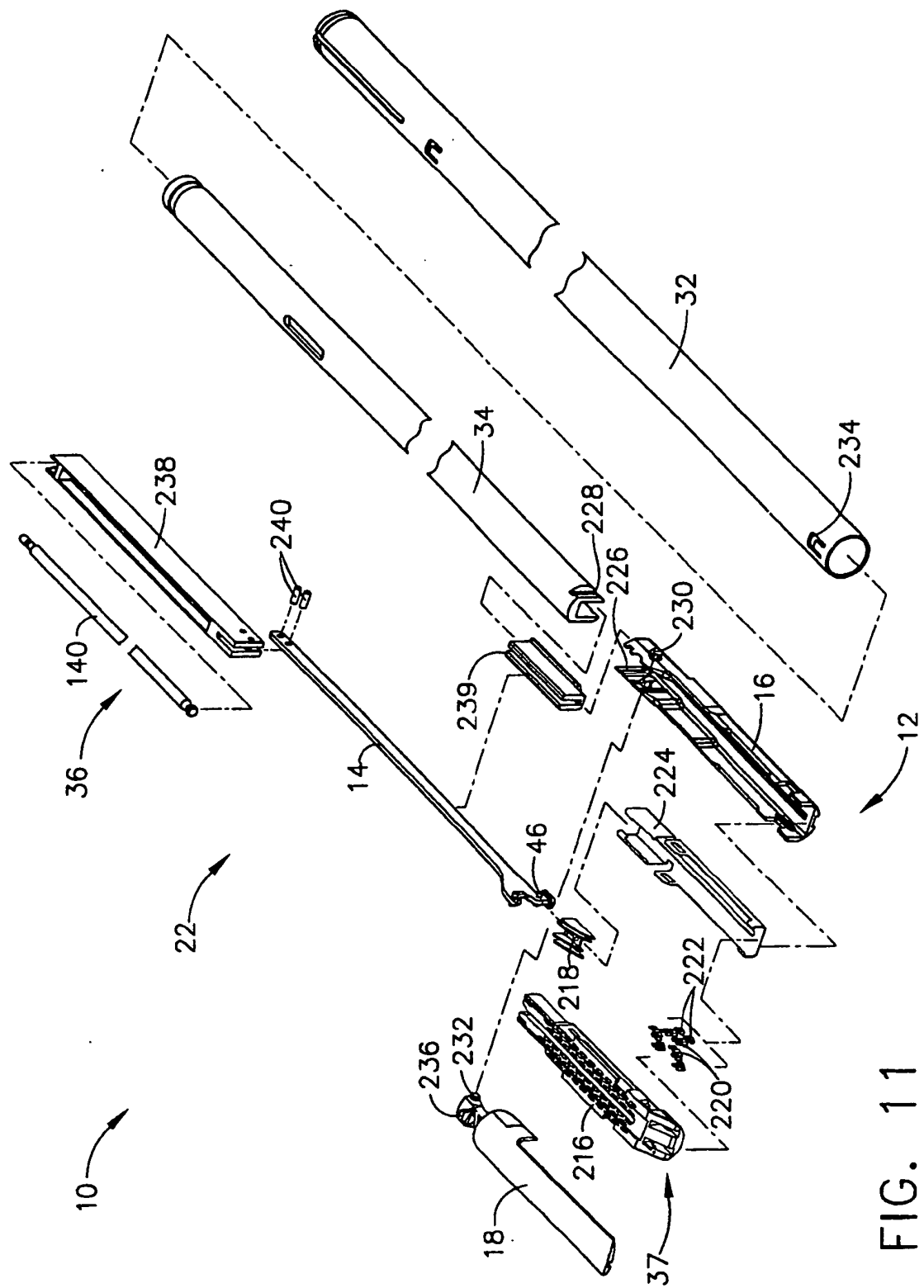
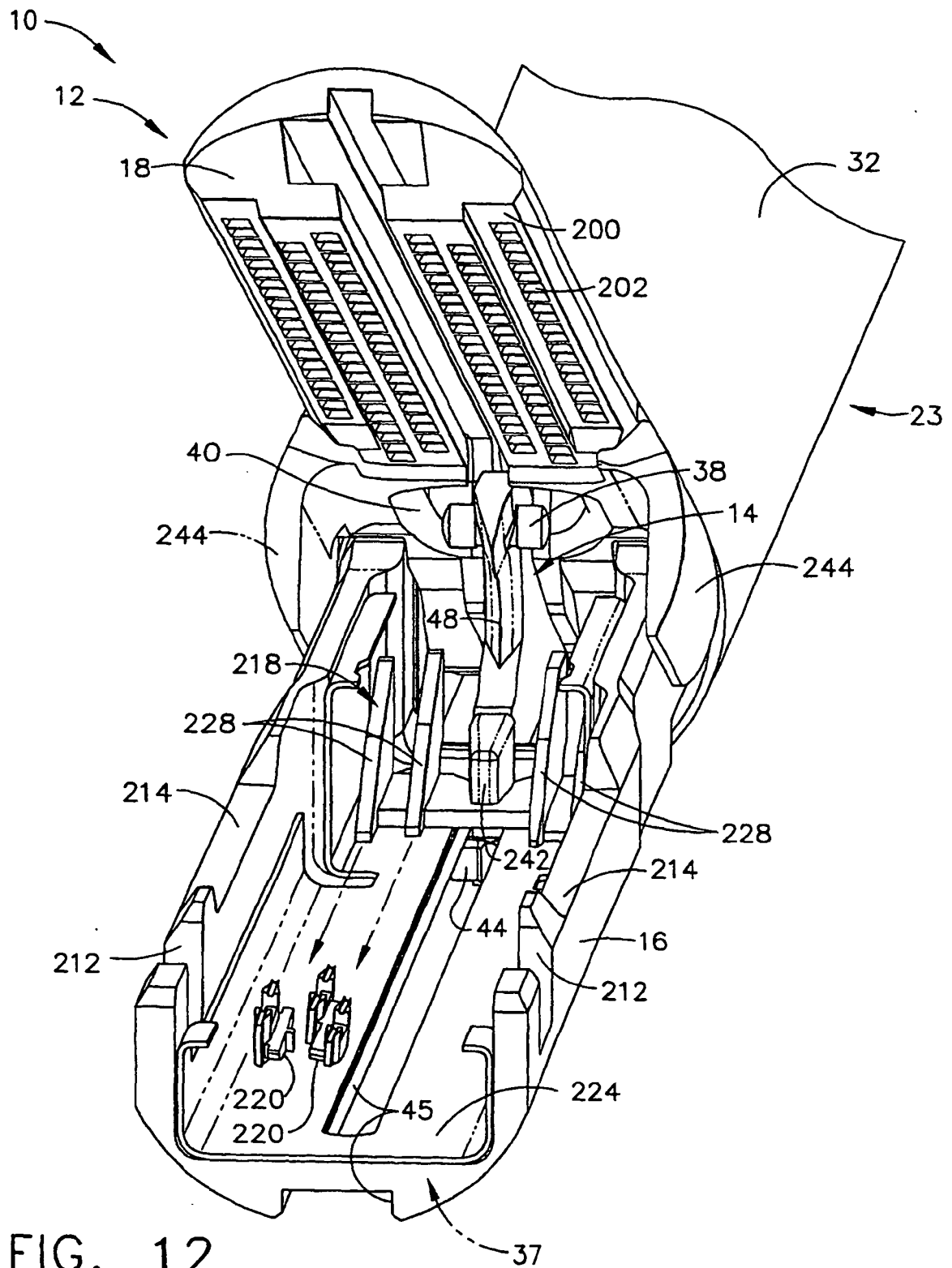


FIG. 11



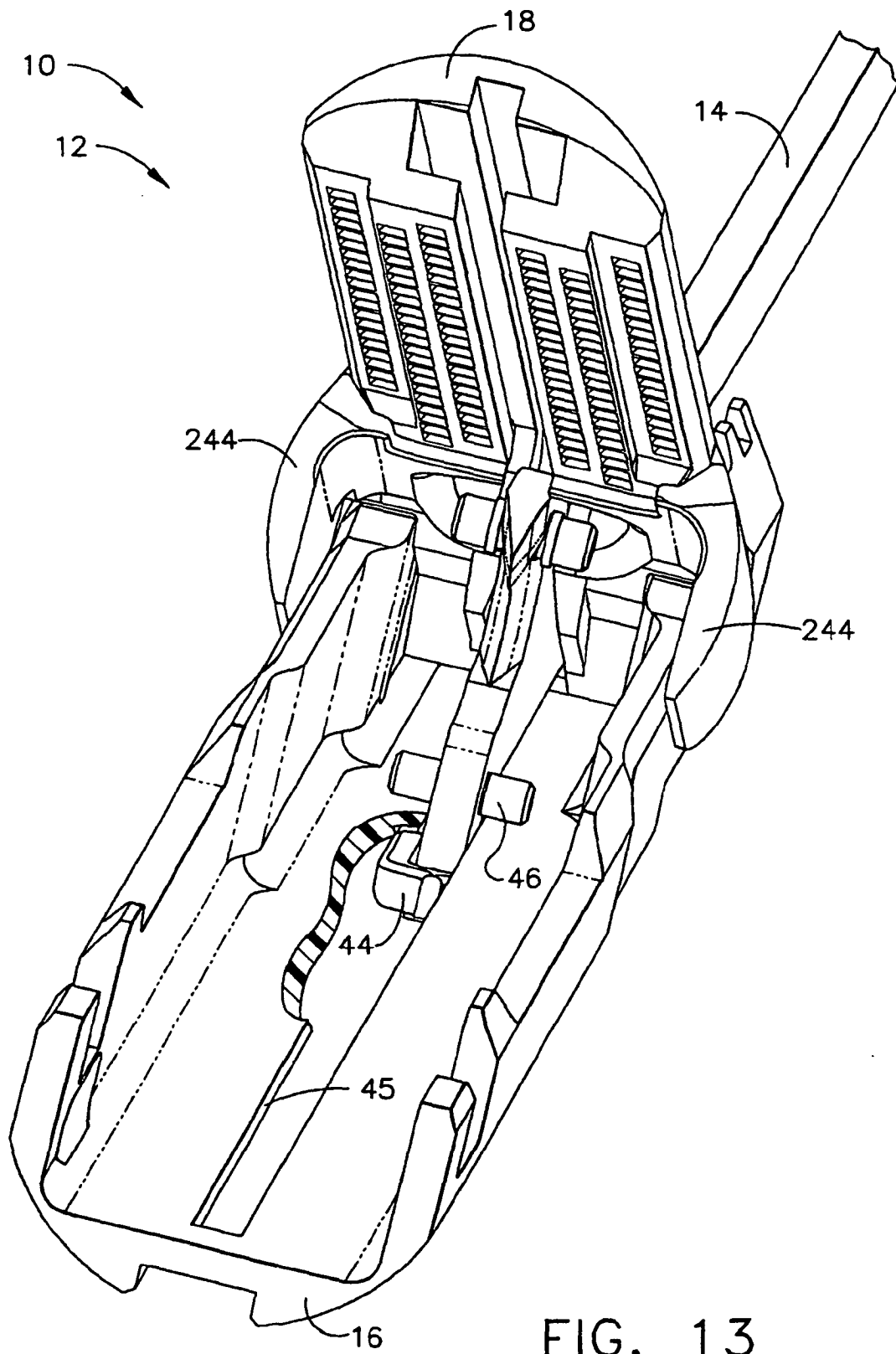


FIG. 13

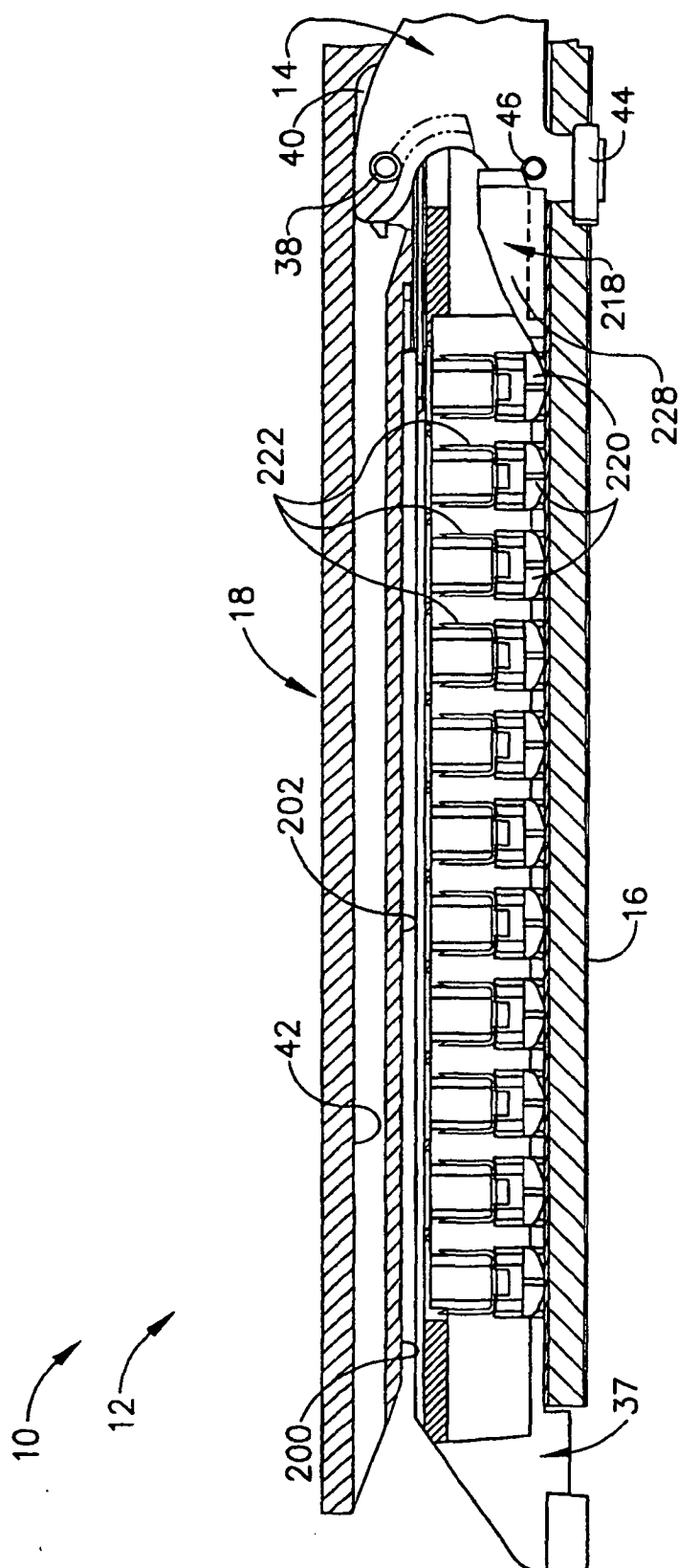


FIG. 14

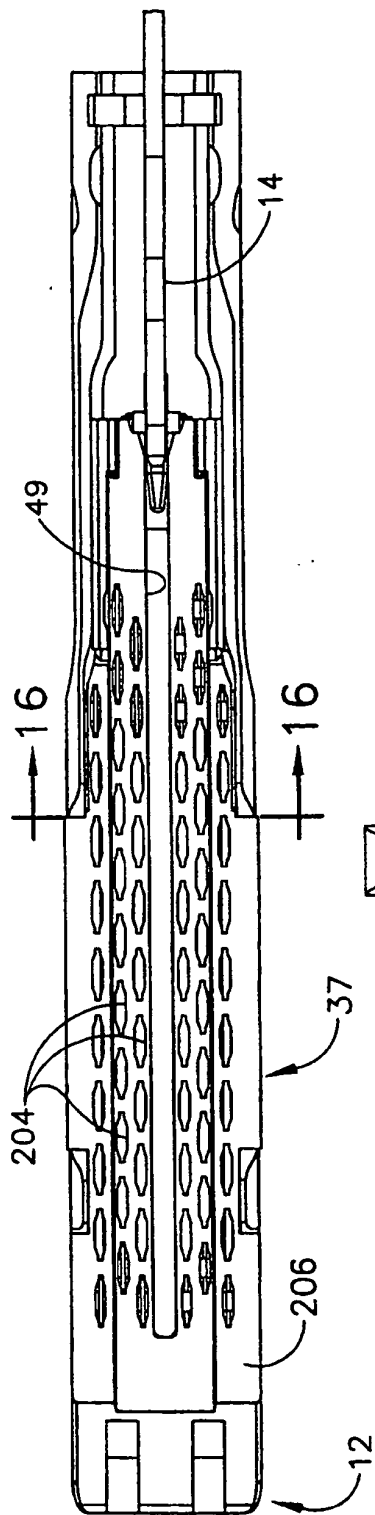


FIG. 15

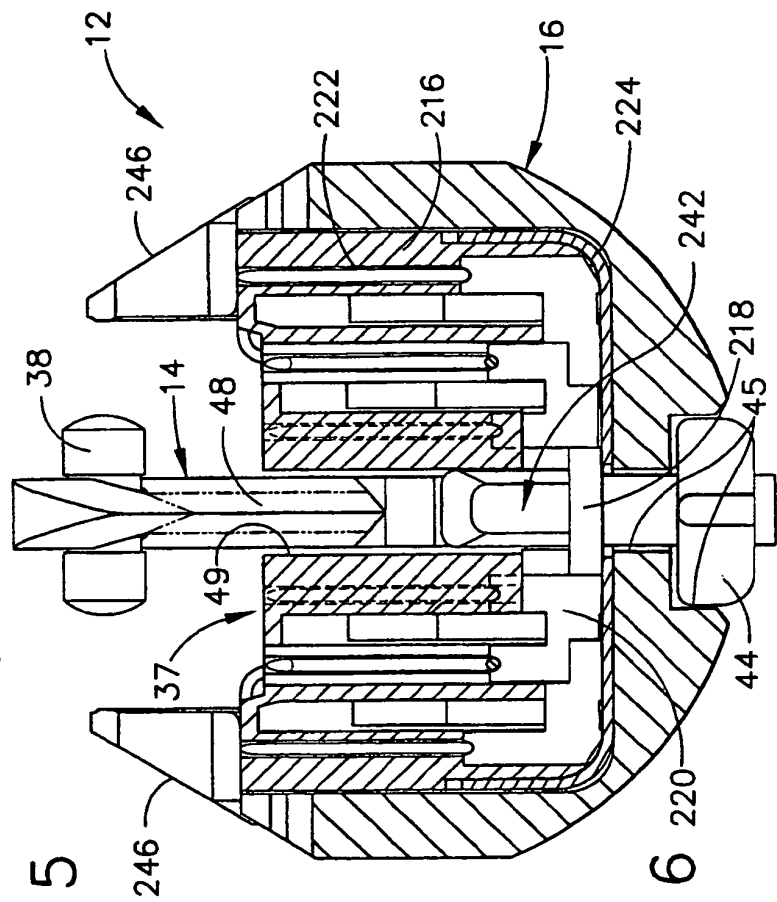


FIG. 16

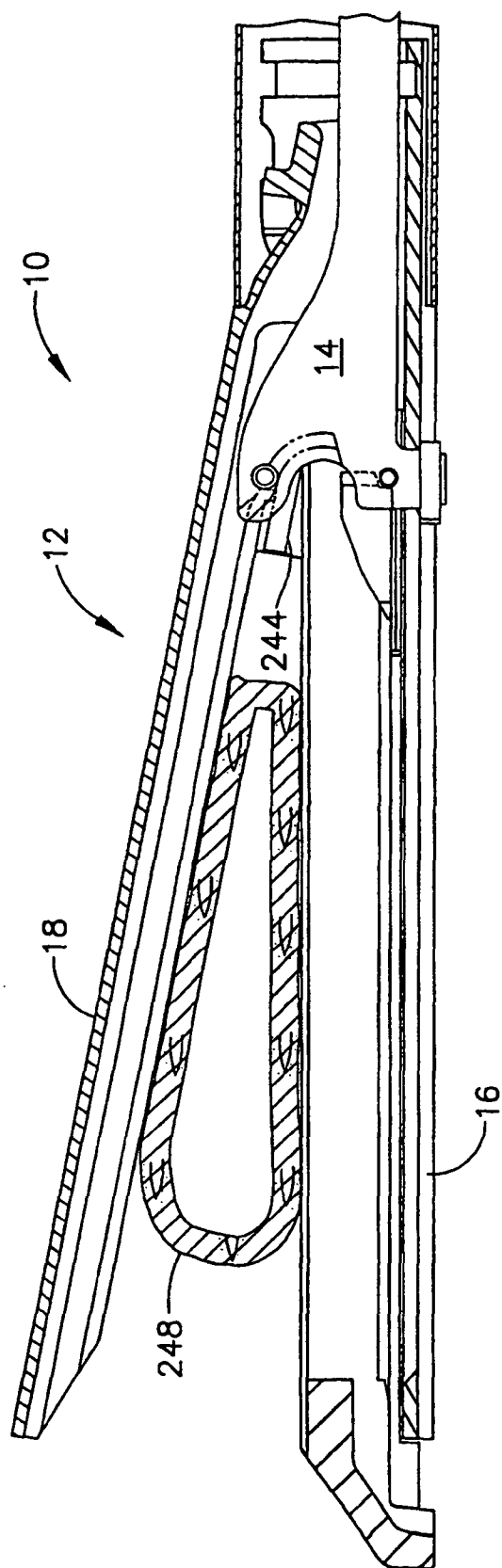


FIG. 17

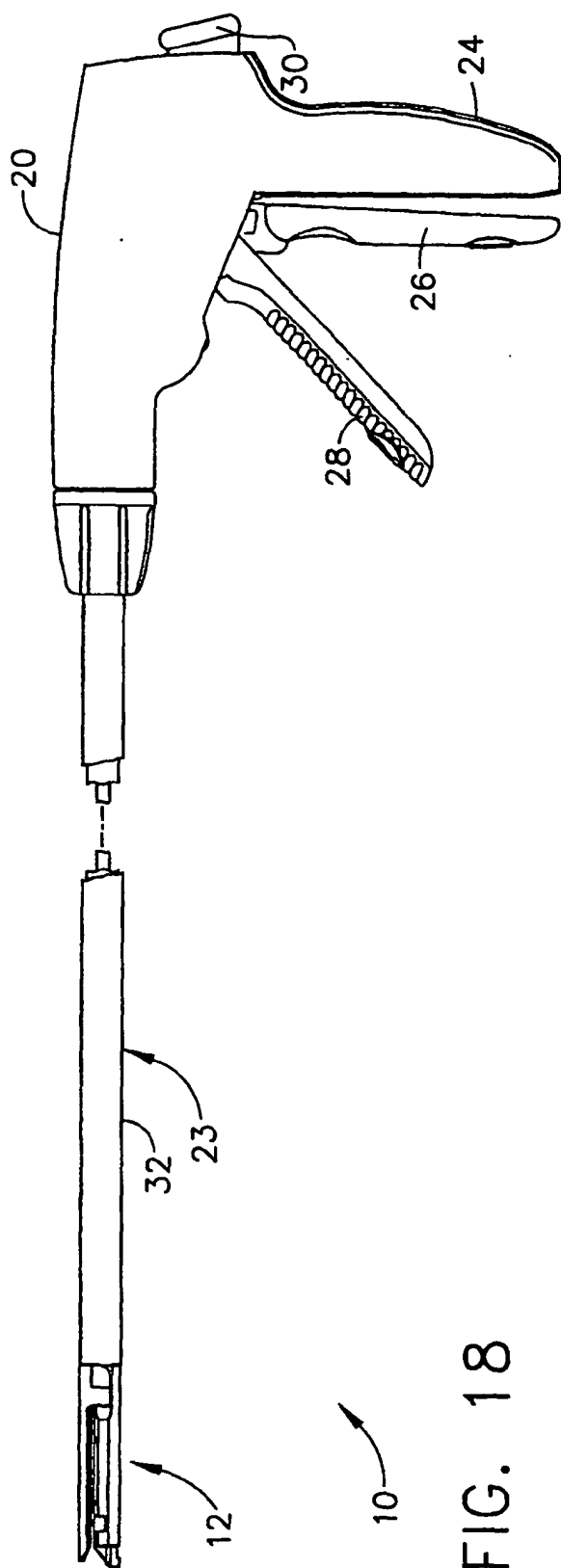


FIG. 18

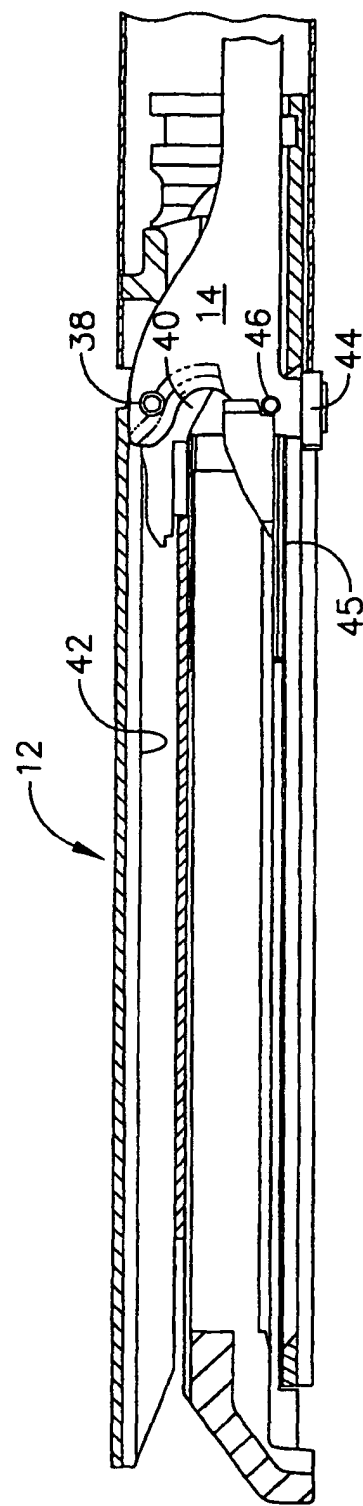


FIG. 19

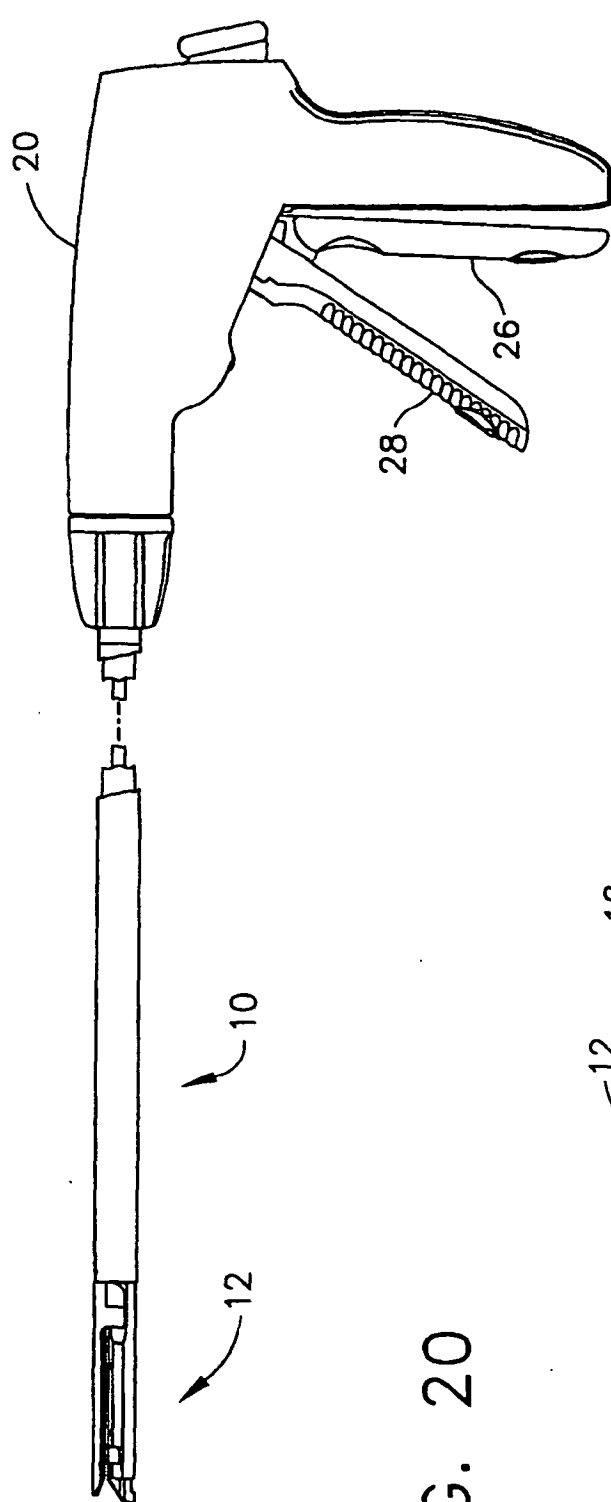


FIG. 20

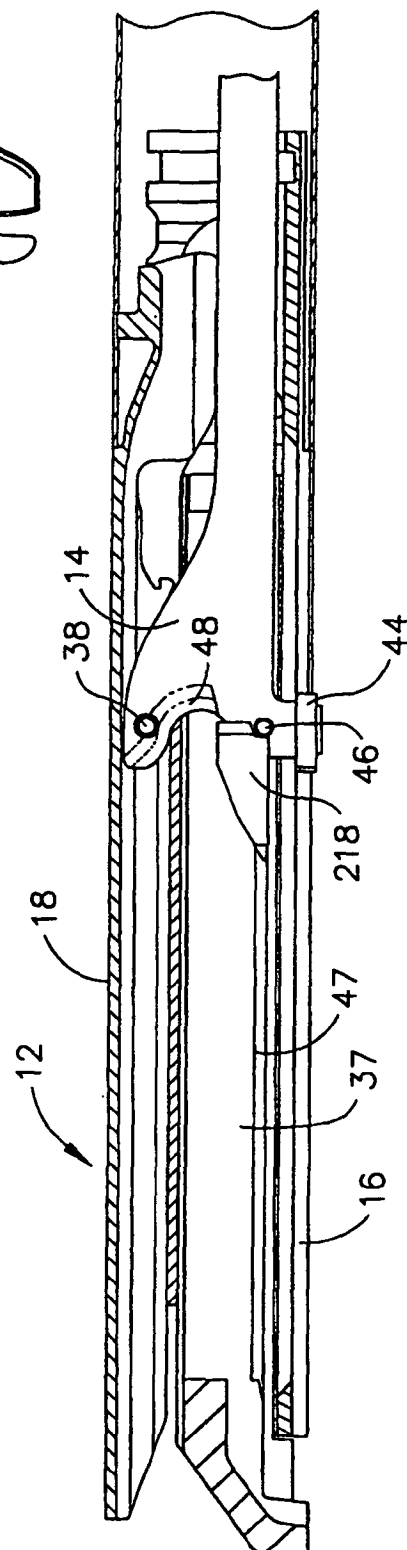


FIG. 21

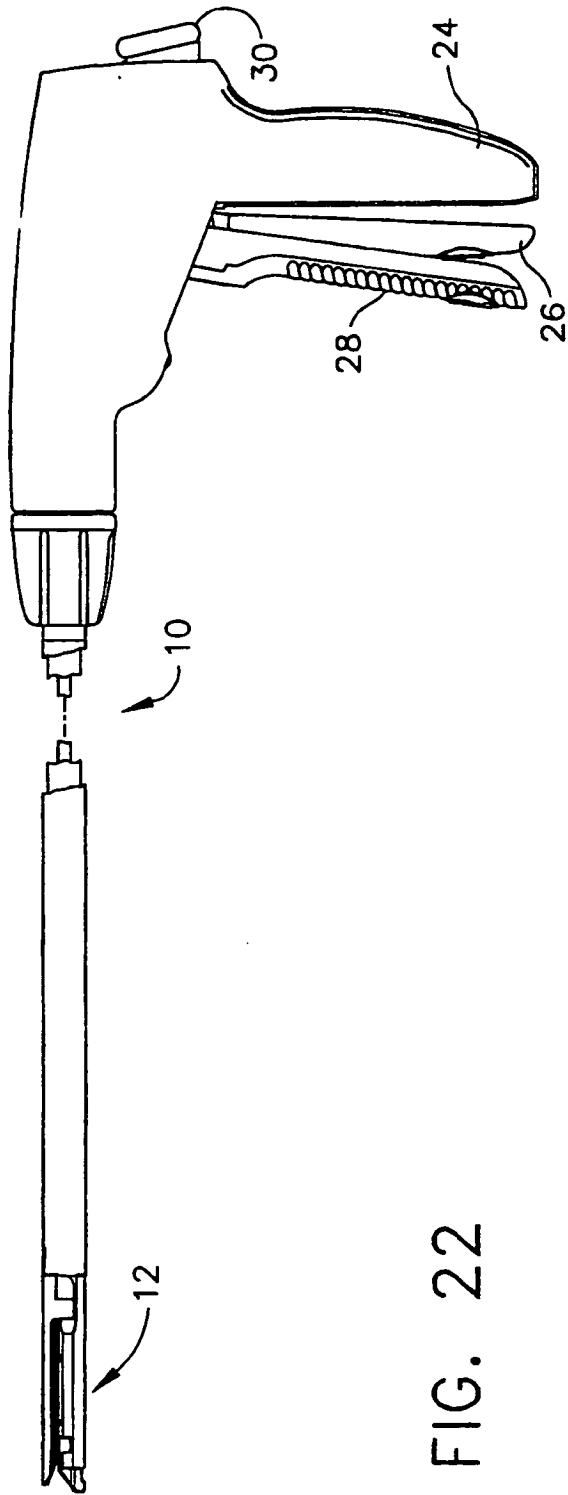


FIG. 22

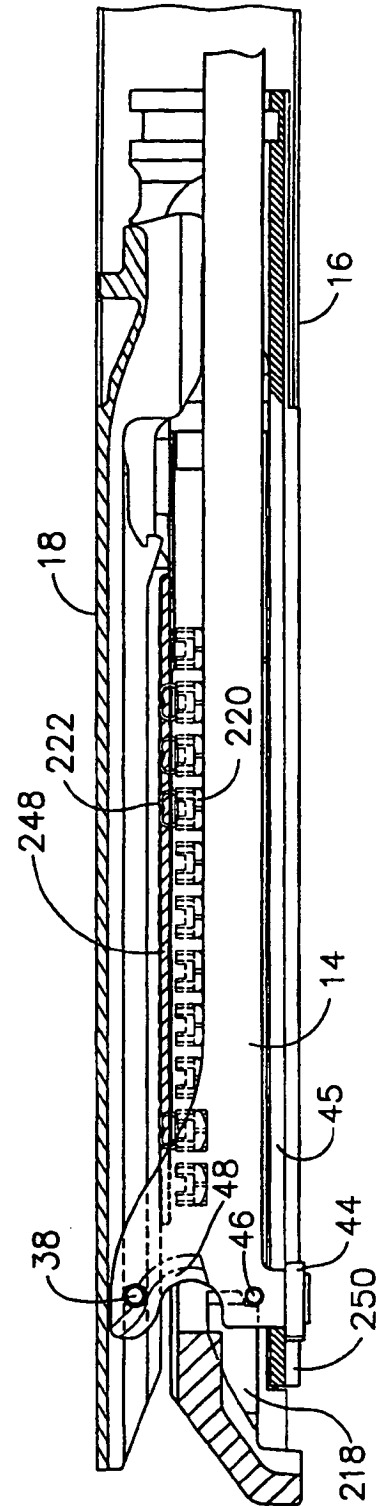


FIG. 23

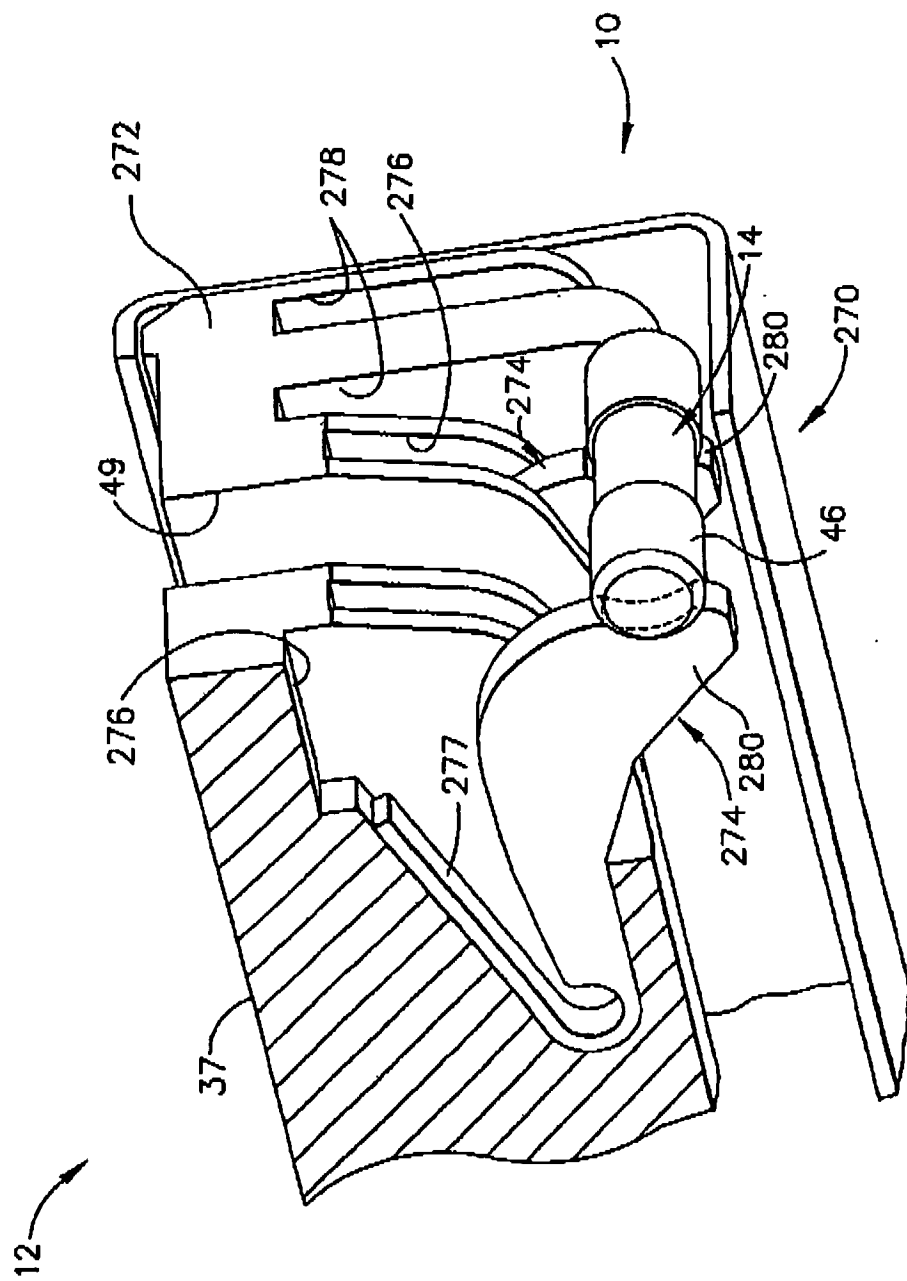


FIG. 24

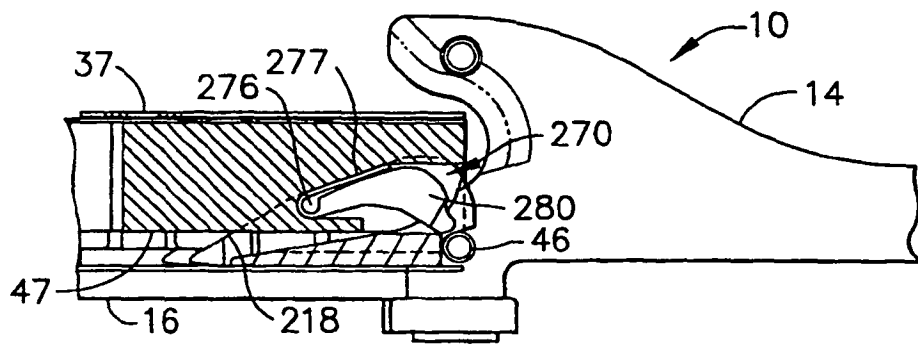


FIG. 25

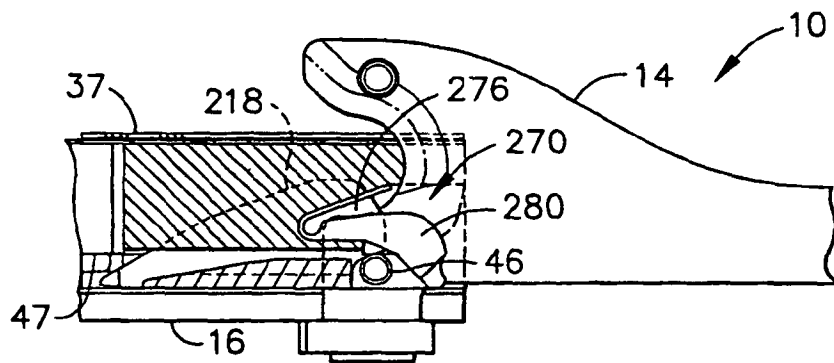


FIG. 26

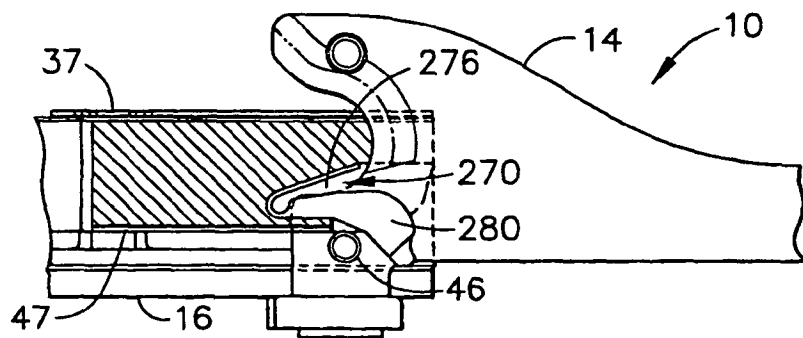


FIG. 27

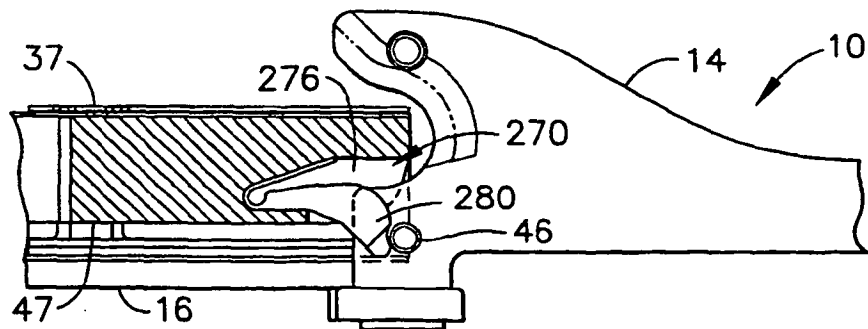


FIG. 28

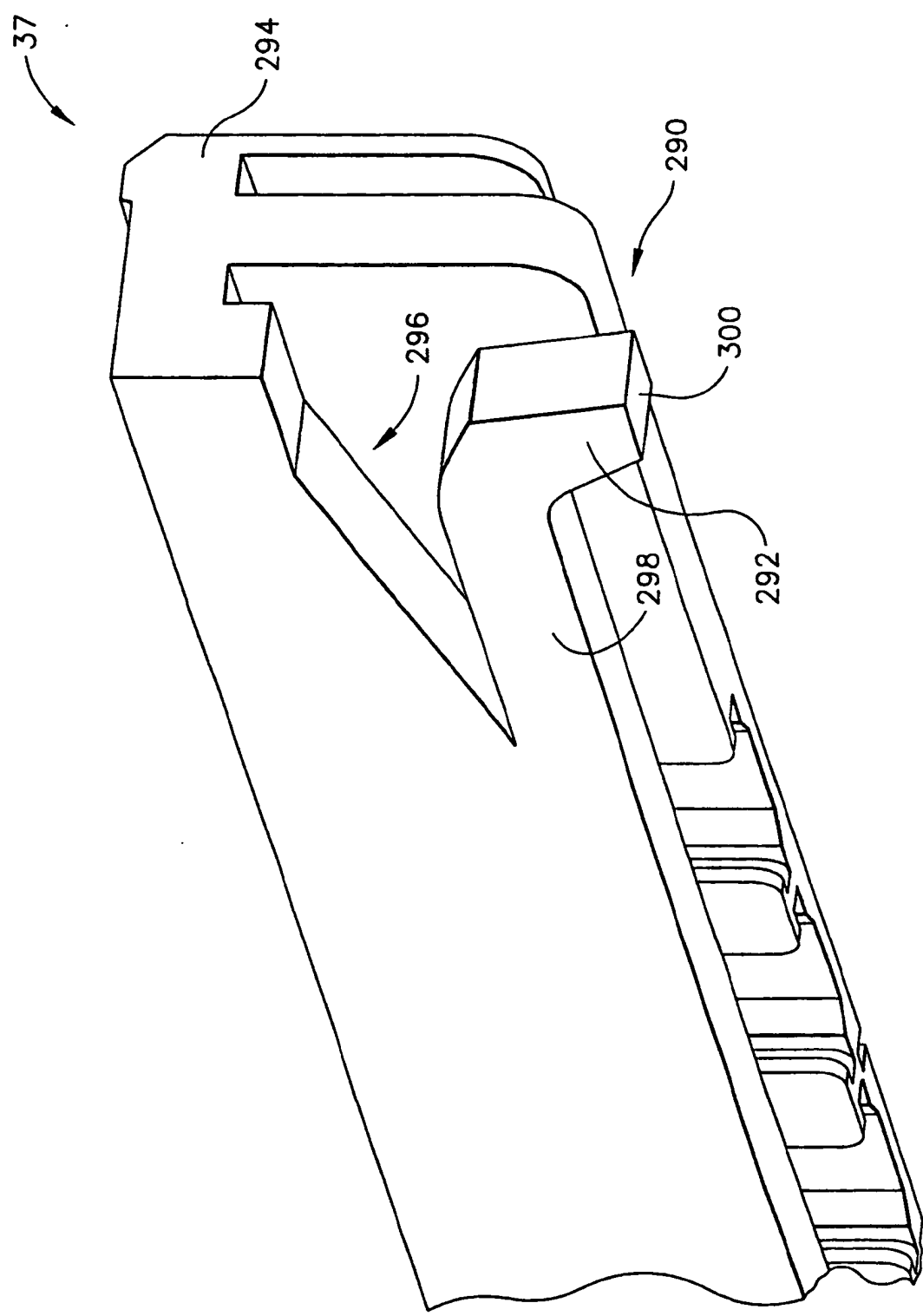


FIG. 29

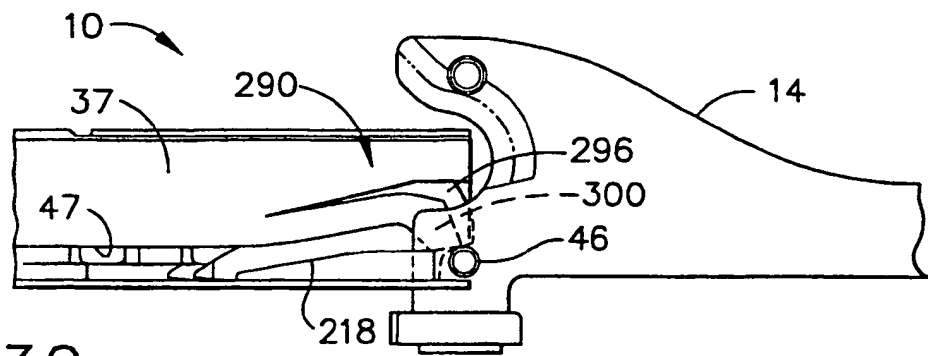


FIG. 30

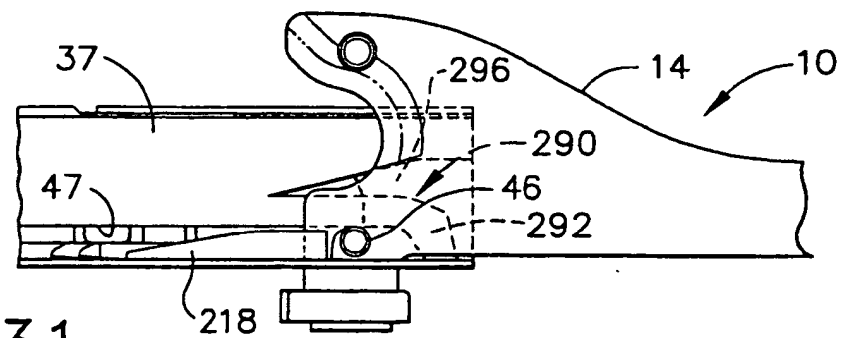


FIG. 31

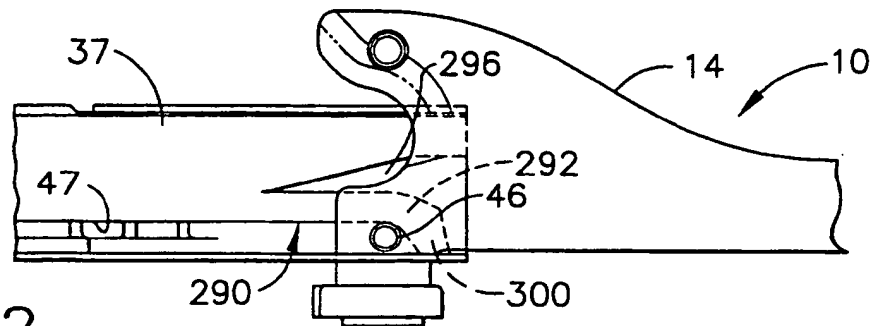


FIG. 32

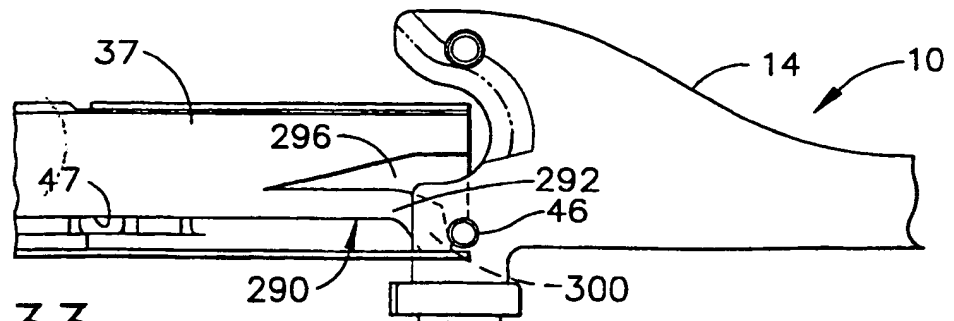


FIG. 33

REFERENCES CITED IN THE DESCRIPTION

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- US 6109500 A [0005]
- WO 03030743 A [0005]

专利名称(译)	具有用过的盒式锁定装置的外科缝合器械		
公开(公告)号	EP1479345B1	公开(公告)日	2008-08-13
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[标]申请(专利权)人(译)	伊西康内外科公司		
申请(专利权)人(译)	爱惜康内镜外科		
当前申请(专利权)人(译)	爱惜康内镜手术，INC.		
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摘要(译)

用于腹腔镜和内窥镜临床手术的外科器械同时切断并缝合夹在末端执行器中的组织，该末端执行器包括保持钉仓的细长通道和枢转连接的砧座。电子束击发杆接合通道并在远侧击发运动期间选择性地接合砧座，其中组织被切断并被钉钉从钉仓向上驱动以形成抵靠砧座。特别地，与钉仓成一体的楔形件由击发杆的中间销向远侧驱动以实现钉合。钉仓的锁定机构响应楔形滑板在其未击发位置的存在，以允许击发杆发射。否则，锁定机构在钉仓用完时防止发射。

