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(54) **Surgical instrument with wireless communication between control unit and remote sensor**

(57) An endoscopic or laparoscopic surgical instrument comprising an end effector (12) having at least one sensor (368) and a control unit (300). The surgical instrument further comprises an electrically conductive shaft (40) having a distal end connected to the end effector. The sensor is electrically insulated from the shaft whereas the control unit is electrically coupled to said shaft (e.g. by link 400) such that the shaft is configured to radiate signals from the control unit to the sensor and to receive radiated signals from the sensor.

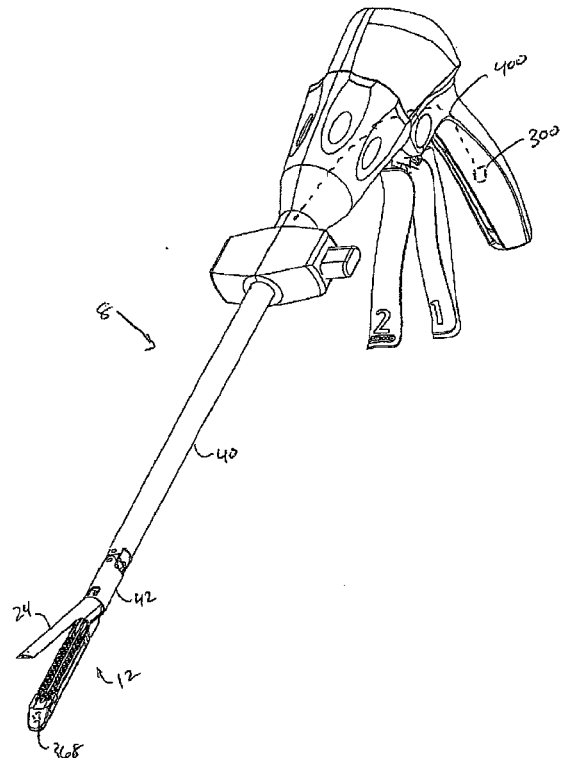


FIG. 16

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Description

CROSS REFERENCE TO RELATED APPLICATIONS

[0001] The present application is related to the following, concurrently-filed U.S. patent applications, which are incorporated herein by reference:

- (1) U.S. Patent Application Serial No. __, entitled "SURGICAL INSTRUMENT WITH WIRELESS COMMUNICATION BETWEEN CONTROL UNIT AND SENSOR TRANSPONDERS," by J. Giordano et al. (Attorney Docket No. 060338/END5923USNP);
- (2) U.S. Patent Application Serial No. __, entitled "SURGICAL INSTRUMENT WITH ELEMENTS TO COMMUNICATE BETWEEN CONTROL UNIT AND END EFFECTOR," by J. Giordano et al. (Attorney Docket No. 060340/END5925USNP);
- (3) U.S. Patent Application Serial No. __, entitled "PREVENTION OF CARTRIDGE REUSE IN A SURGICAL INSTRUMENT," by F. Shelton et al. (Attorney Docket No. 060341/END5926USNP);
- (4) U.S. Patent Application Serial No. __, entitled "POST-STERILIZATION PROGRAMMING OF SURGICAL INSTRUMENTS," by J. Swayze et al. (Attorney Docket No. 060342/END5924USNP);
- (5) U.S. Patent Application Serial No. __, entitled "INTERLOCK AND SURGICAL INSTRUMENT INCLUDING SAME," by F. Shelton et al. (Attorney Docket No. 060343/END5928USNP); and
- (6) U.S. Patent Application Serial No. __, entitled "SURGICAL INSTRUMENT WITH ENHANCED BATTERY PERFORMANCE," by F. Shelton et al. (Attorney Docket No. 060347/END5931USNP).

BACKGROUND

[0002] Endoscopic surgical instruments are often preferred over traditional open surgical devices since a smaller incision tends to reduce the post-operative recovery time and complications. Consequently, significant development has gone into a range of endoscopic surgical instruments that are suitable for precise placement of a distal end effector at a desired surgical site through a cannula of a trocar. These distal end effectors engage the tissue in a number of ways to achieve a diagnostic or therapeutic effect (e.g., endocutter, grasper, cutter, staplers, clip applier, access device, drug/gene therapy delivery device, and energy device using ultrasound, RF, laser, etc.).

[0003] Known surgical staplers include an end effector that simultaneously makes a longitudinal incision in tissue and applies lines of staples on opposing sides of the incision. The end effector includes a pair of cooperating jaw members that, if the instrument is intended for endoscopic or laparoscopic applications, are capable of passing through a cannula passageway. One of the jaw members receives a staple cartridge having at least two lat-

erally spaced rows of staples. The other jaw member defines an anvil having staple-forming pockets aligned with the rows of staples in the cartridge. The instrument includes a plurality of reciprocating wedges which, when driven distally, pass through openings in the staple cartridge and engage drivers supporting the staples to effect the firing of the staples toward the anvil.

[0004] An example of a surgical stapler suitable for endoscopic applications is described in U.S. Pat. No. 5,465,895, which discloses an endocutter with distinct closing and firing actions. A clinician using this device is able to close the jaw members upon tissue to position the tissue prior to firing. Once the clinician has determined that the jaw members are properly gripping tissue, the clinician can then fire the surgical stapler with a single firing stroke, thereby severing and stapling the tissue. The simultaneous severing and stapling avoids complications that may arise when performing such actions sequentially with different surgical tools that respectively only sever and staple.

[0005] One specific advantage of being able to close upon tissue before firing is that the clinician is able to verify via an endoscope that the desired location for the cut has been achieved, including that a sufficient amount of tissue has been captured between opposing jaws. Otherwise, opposing jaws may be drawn too close together, especially pinching at their distal ends, and thus not effectively forming closed staples in the severed tissue. At the other extreme, an excessive amount of clamped tissue may cause binding and an incomplete firing.

[0006] Endoscopic staplers/cutters continue to increase in complexity and function with each generation. One of the main reasons for this is the quest to lower force-to-fire (FTF) to a level that all or a great majority of surgeons can handle. One known solution to lower FTF is to use CO₂ or electrical motors. These devices have not fared much better than traditional hand-powered devices, but for a different reason. Surgeons typically prefer to experience proportionate force distribution to that being experienced by the end effector in the forming of the staple to assure them that the cutting/stapling cycle is complete, with the upper limit within the capabilities of most surgeons (usually around 15-30 lbs). They also typically want to maintain control of deploying the staples and being able to stop at anytime if the forces felt in the handle of the device feel too great or for some other clinical reason.

[0007] To address this need, so-called "power-assist" endoscopic surgical instruments have been developed in which a supplemental power source aids in the firing of the instrument. For example, in some power-assist devices, a motor provides supplemental electrical power to the power input by the user from squeezing the firing trigger. Such devices are capable of providing loading force feedback and control to the operator to reduce the firing force required to be exerted by the operator in order to complete the cutting operation. One such power-assist device is described in United States Patent Application

Serial No. 11/343,573, filed January 31, 2006 by Shelton et al., entitled "Motor-driven surgical cutting and fastening instrument with loading force feedback," ("the '573 application") which is incorporated herein by reference.

[0008] These power-assist devices often include other components that purely mechanical endoscopic surgical instruments do not, such as sensors and control systems. One challenge in using such electronics in a surgical instrument is delivering power and/or data to and from the sensors, particularly when there is a free rotating joint in the surgical instrument.

SUMMARY

[0009] In one general aspect, the present invention is directed to a surgical instrument, such as an endoscopic or laparoscopic instrument. According to one embodiment, the surgical instrument comprises an end effector comprising at least one sensor transponder that is passively powered. The surgical instrument also comprises a shaft having a distal end connected to the end effector and a handle connected to a proximate end of the shaft. The handle comprises a control unit (e.g., a microcontroller) that is in communication with the sensor transponder via at least one inductive coupling. Further, the surgical instrument may comprise a rotational joint for rotating the shaft. In such a case, the surgical instrument may comprise a first inductive element located in the shaft distally from the rotational joint and inductively coupled to the control unit, and a second inductive element located distally in the shaft and inductively coupled to the at least one sensor transponder. The first and second inductive elements may be connected by a wired, physical connection.

[0010] That way, the control unit may communicate with the transponder in the end effector without a direct wired connection through complex mechanical joints like the rotating joint where it may be difficult to maintain such a wired connection. In addition, because the distances between the inductive elements may be fixed and known, the couplings could be optimized for inductive transfer of energy. Also, the distances could be relatively short so that relatively low power signals could be used to thereby minimize interference with other systems in the use environment of the instrument.

[0011] In another general aspect of the present invention, the electrically conductive shaft of the surgical instrument may serve as an antenna for the control unit to wirelessly communicate signals to and from the sensor transponder. For example, the sensor transponder could be located on or disposed in a nonconductive component of the end effector, such as a plastic cartridge, thereby insulating the sensor from conductive components of the end effector and the shaft. In addition, the control unit in the handle may be electrically coupled to the shaft. In that way, the shaft and/or the end effector may serve as an antenna for the control unit by radiating signals from the control unit to the sensor and/or by receiving radiated

signals from the sensor. Such a design is particularly useful in surgical instruments having complex mechanical joints (such as rotary joints), which make it difficult to use a direct wired connection between the sensor and control unit for communicating data signals.

[0012] In another embodiment, the shaft and/or components of the end effector could serve as the antenna for the sensor by radiating signals to the control unit and receiving radiated signals from the control unit. According to such an embodiment, the control unit is electrically insulated from the shaft and the end effector.

[0013] In another general aspect, the present invention is directed to a surgical instrument comprising a programmable control unit that can be programmed by a programming device after the instrument has been packaged and sterilized. In one such embodiment, the programming device may wirelessly program the control unit. The control unit may be passively powered by the wireless signals from the programming device during the programming operation. In another embodiment, the sterile container may comprise a connection interface so that the programming unit can be connected to the surgical instrument while the surgical instrument is in its sterilized container.

FIGURES

[0014] Various embodiments of the present invention are described herein by way of example in conjunction with the following figures wherein:

Figures 1 and 2 are perspective views of a surgical instrument according to various embodiments of the present invention;

Figures 3-5 are exploded views of an end effector and shaft of the instrument according to various embodiments of the present invention;

Figure 6 is a side view of the end effector according to various embodiments of the present invention;

Figure 7 is an exploded view of the handle of the instrument according to various embodiments of the present invention;

Figures 8 and 9 are partial perspective views of the handle according to various embodiments of the present invention;

Figure 10 is a side view of the handle according to various embodiments of the present invention;

Figures 11, 13-14, 16, and 22 are perspective views of a surgical instrument according to various embodiments of the present invention;

Figures 12 and 19 are block diagrams of a control unit according to various embodiments of the present invention;

Figure 15 is a side view of an end effector including a sensor transponder according to various embodiments of the present invention;

Figures 17 and 18 show the instrument in a sterile container according to various embodiments of the

present invention;

Figure 20 is a block diagram of the remote programming device according to various embodiments of the present invention; and

Figure 21 is a diagram of a packaged instrument according to various embodiments of the present invention.

DETAILED DESCRIPTION

[0015] Various embodiments of the present invention are directed generally to a surgical instrument having at least one remote sensor transponder and means for communicating power and/or data signals to the transponder (s) from a control unit. The present invention may be used with any type of surgical instrument comprising at least one sensor transponder, such as endoscopic or laparoscopic surgical instruments, but is particularly useful for surgical instruments where some feature of the instrument, such as a free rotating joint, prevents or otherwise inhibits the use of a wired connection to the sensor(s). Before describing aspects of the system, one type of surgical instrument in which embodiments of the present invention may be used - an endoscopic stapling and cutting instrument (i.e., an endocutter) - is first described by way of illustration.

[0016] Figures 1 and 2 depict an endoscopic surgical instrument 10 that comprises a handle 6, a shaft 8, and an articulating end effector 12 pivotally connected to the shaft 8 at an articulation pivot 14. Correct placement and orientation of the end effector 12 may be facilitated by controls on the handle 6, including (1) a rotation knob 28 for rotating the closure tube (described in more detail below in connection with Figures 4-5) at a free rotating joint 29 of the shaft 8 to thereby rotate the end effector 12 and (2) an articulation control 16 to effect rotational articulation of the end effector 12 about the articulation pivot 14. In the illustrated embodiment, the end effector 12 is configured to act as an endocutter for clamping, severing and stapling tissue, although in other embodiments, different types of end effectors may be used, such as end effectors for other types of surgical instruments, such as graspers, cutters, staplers, clip applicators, access devices, drug/gene therapy devices, ultrasound, RF or laser devices, etc.

[0017] The handle 6 of the instrument 10 may include a closure trigger 18 and a firing trigger 20 for actuating the end effector 12. It will be appreciated that instruments having end effectors directed to different surgical tasks may have different numbers or types of triggers or other suitable controls for operating the end effector 12. The end effector 12 is shown separated from the handle 6 by the preferably elongate shaft 8. In one embodiment, a clinician or operator of the instrument 10 may articulate the end effector 12 relative to the shaft 8 by utilizing the articulation control 16, as described in more detail in pending U.S. patent application Ser. No. 11/329,020, filed January 10, 2006, entitled "Surgical Instrument Hav-

ing An Articulating End Effector," by Geoffrey C. Hueil et al., which is incorporated herein by reference.

[0018] The end effector 12 includes in this example, among other things, a staple channel 22 and a pivotally translatable clamping member, such as an anvil 24, which are maintained at a spacing that assures effective stapling and severing of tissue clamped in the end effector 12. The handle 6 includes a pistol grip 26 towards which a closure trigger 18 is pivotally drawn by the clinician to cause clamping or closing of the anvil 24 toward the staple channel 22 of the end effector 12 to thereby clamp tissue positioned between the anvil 24 and channel 22. The firing trigger 20 is farther outboard of the closure trigger 18. Once the closure trigger 18 is locked in the closure position, the firing trigger 20 may rotate slightly toward the pistol grip 26 so that it can be reached by the operator using one hand. Then the operator may pivotally draw the firing trigger 20 toward the pistol grip 12 to cause the stapling and severing of clamped tissue in the end effector 12. The '573 application describes various configurations for locking and unlocking the closure trigger 18. In other embodiments, different types of clamping members besides the anvil 24 could be used, such as, for example, an opposing jaw, etc.

[0019] It will be appreciated that the terms "proximal" and "distal" are used herein with reference to a clinician gripping the handle 6 of an instrument 10. Thus, the end effector 12 is distal with respect to the more proximal handle 6. It will be further appreciated that, for convenience and clarity, spatial terms such as "vertical" and "horizontal" are used herein with respect to the drawings. However, surgical instruments are used in many orientations and positions, and these terms are not intended to be limiting and absolute.

[0020] The closure trigger 18 may be actuated first. Once the clinician is satisfied with the positioning of the end effector 12, the clinician may draw back the closure trigger 18 to its fully closed, locked position proximate to the pistol grip 26. The firing trigger 20 may then be actuated. The firing trigger 20 returns to the open position (shown in Figures 1 and 2) when the clinician removes pressure. A release button 30 on the handle 6, and in this example, on the pistol grip 26 of the handle, when depressed may release the locked closure trigger 18.

[0021] Figure 3 is an exploded view of the end effector 12 according to various embodiments. As shown in the illustrated embodiment, the end effector 12 may include, in addition to the previously-mentioned channel 22 and anvil 24, a cutting instrument 32, a sled 33, a staple cartridge 34 that is removably seated in the channel 22, and a helical screw shaft 36. The cutting instrument 32 may be, for example, a knife. The anvil 24 may be pivotally opened and closed at a pivot point 25 connected to the proximate end of the channel 22. The anvil 24 may also include a tab 27 at its proximate end that is inserted into a component of the mechanical closure system (described further below) to open and close the anvil 24. When the closure trigger 18 is actuated, that is, drawn in

by a user of the instrument 10, the anvil 24 may pivot about the pivot point 25 into the clamped or closed position. If clamping of the end effector 12 is satisfactory, the operator may actuate the firing trigger 20, which, as explained in more detail below, causes the knife 32 and sled 33 to travel longitudinally along the channel 22, thereby cutting tissue clamped within the end effector 12. The movement of the sled 33 along the channel 22 causes the staples of the staple cartridge 34 to be driven through the severed tissue and against the closed anvil 24, which turns the staples to fasten the severed tissue. U.S. Pat. 6,978,921, entitled "Surgical stapling instrument incorporating an E-beam firing mechanism," which is incorporated herein by reference, provides more details about such two-stroke cutting and fastening instruments. The sled 33 may be part of the cartridge 34, such that when the knife 32 retracts following the cutting operation, the sled 33 does not retract. The channel 22 and the anvil 24 may be made of an electrically conductive material (such as metal) so that they may serve as part of the antenna that communicates with the sensor(s) in the end effector, as described further below. The cartridge 34 could be made of a nonconductive material (such as plastic) and the sensor may be connected to or disposed in the cartridge 34, as described further below.

[0022] It should be noted that although the embodiments of the instrument 10 described herein employ an end effector 12 that staples the severed tissue, in other embodiments different techniques for fastening or sealing the severed tissue may be used. For example, end effectors that use RF energy or adhesives to fasten the severed tissue may also be used. U.S. Patent No. 5,709,680, entitled "Electrosurgical Hemostatic Device" to Yates et al., and U.S. Patent No. 5,688,270, entitled "Electrosurgical Hemostatic Device With Recessed And/Or Offset Electrodes" to Yates et al., which are incorporated herein by reference, discloses cutting instruments that use RF energy to fasten the severed tissue. U.S. Patent Application Serial No. 11/267,811 to Morgan et al. and U.S. Patent Application Serial No. 11/267,363 to Shelton et al., which are also incorporated herein by reference, disclose cutting instruments that use adhesives to fasten the severed tissue. Accordingly, although the description herein refers to cutting/stapling operations and the like, it should be recognized that this is an exemplary embodiment and is not meant to be limiting. Other tissue-fastening techniques may also be used.

[0023] Figures 4 and 5 are exploded views and Figure 6 is a side view of the end effector 12 and shaft 8 according to various embodiments. As shown in the illustrated embodiment, the shaft 8 may include a proximate closure tube 40 and a distal closure tube 42 pivotably linked by a pivot links 44. The distal closure tube 42 includes an opening 45 into which the tab 27 on the anvil 24 is inserted in order to open and close the anvil 24. Disposed inside the closure tubes 40, 42 may be a proximate spine tube 46. Disposed inside the proximate spine tube 46 may be a main rotational (or proximate) drive shaft 48 that com-

municates with a secondary (or distal) drive shaft 50 via a bevel gear assembly 52. The secondary drive shaft 50 is connected to a drive gear 54 that engages a proximate drive gear 56 of the helical screw shaft 36. The vertical bevel gear 52b may sit and pivot in an opening 57 in the distal end of the proximate spine tube 46. A distal spine tube 58 may be used to enclose the secondary drive shaft 50 and the drive gears 54, 56. Collectively, the main drive shaft 48, the secondary drive shaft 50, and the articulation assembly (e.g., the bevel gear assembly 52a-c), are sometimes referred to herein as the "main drive shaft assembly." The closure tubes 40, 42 may be made of electrically conductive material (such as metal) so that they may serve as part of the antenna, as described further below. Components of the main drive shaft assembly (e.g., the drive shafts 48, 50) may be made of a nonconductive material (such as plastic).

[0024] A bearing 38, positioned at a distal end of the staple channel 22, receives the helical drive screw 36, allowing the helical drive screw 36 to freely rotate with respect to the channel 22. The helical screw shaft 36 may interface a threaded opening (not shown) of the knife 32 such that rotation of the shaft 36 causes the knife 32 to translate distally or proximally (depending on the direction of the rotation) through the staple channel 22. Accordingly, when the main drive shaft 48 is caused to rotate by actuation of the firing trigger 20 (as explained in more detail below), the bevel gear assembly 52a-c causes the secondary drive shaft 50 to rotate, which in turn, because of the engagement of the drive gears 54, 56, causes the helical screw shaft 36 to rotate, which causes the knife 32 to travel longitudinally along the channel 22 to cut any tissue clamped within the end effector. The sled 33 may be made of, for example, plastic, and may have a sloped distal surface. As the sled 33 traverses the channel 22, the sloped forward surface may push up or drive the staples in the staple cartridge 34 through the clamped tissue and against the anvil 24. The anvil 24 turns the staples, thereby stapling the severed tissue. When the knife 32 is retracted, the knife 32 and sled 33 may become disengaged, thereby leaving the sled 33 at the distal end of the channel 22.

[0025] According to various embodiments, as shown Figures 7-10, the surgical instrument may include a battery 64 in the handle 6. The illustrated embodiment provides user-feedback regarding the deployment and loading force of the cutting instrument in the end effector 12. In addition, the embodiment may use power provided by the user in retracting the firing trigger 18 to power the instrument 10 (a so-called "power assist" mode). As shown in the illustrated embodiment, the handle 6 includes exterior lower side pieces 59, 60 and exterior upper side pieces 61, 62 that fit together to form, in general, the exterior of the handle 6. The handle pieces 59-62 may be made of an electrically nonconductive material, such as plastic. A battery 64 may be provided in the pistol grip portion 26 of the handle 6. The battery 64 powers a motor 65 disposed in an upper portion of the pistol grip

portion 26 of the handle 6. The battery 64 may be constructed according to any suitable construction or chemistry including, for example, a Li-ion chemistry such as LiCoO_2 or LiNiO_2 , a Nickel Metal Hydride chemistry, etc. According to various embodiments, the motor 65 may be a DC brushed driving motor having a maximum rotation of, approximately, 5000 RPM to 100,000 RPM. The motor 64 may drive a 90° bevel gear assembly 66 comprising a first bevel gear 68 and a second bevel gear 70. The bevel gear assembly 66 may drive a planetary gear assembly 72. The planetary gear assembly 72 may include a pinion gear 74 connected to a drive shaft 76. The pinion gear 74 may drive a mating ring gear 78 that drives a helical gear drum 80 via a drive shaft 82. A ring 84 may be threaded on the helical gear drum 80. Thus, when the motor 65 rotates, the ring 84 is caused to travel along the helical gear drum 80 by means of the interposed bevel gear assembly 66, planetary gear assembly 72 and ring gear 78.

[0026] The handle 6 may also include a run motor sensor 110 in communication with the firing trigger 20 to detect when the firing trigger 20 has been drawn in (or "closed") toward the pistol grip portion 26 of the handle 6 by the operator to thereby actuate the cutting/stapling operation by the end effector 12. The sensor 110 may be a proportional sensor such as, for example, a rheostat or variable resistor. When the firing trigger 20 is drawn in, the sensor 110 detects the movement, and sends an electrical signal indicative of the voltage (or power) to be supplied to the motor 65. When the sensor 110 is a variable resistor or the like, the rotation of the motor 65 may be generally proportional to the amount of movement of the firing trigger 20. That is, if the operator only draws or closes the firing trigger 20 in a little bit, the rotation of the motor 65 is relatively low. When the firing trigger 20 is fully drawn in (or in the fully closed position), the rotation of the motor 65 is at its maximum. In other words, the harder the user pulls on the firing trigger 20, the more voltage is applied to the motor 65, causing greater rates of rotation. In another embodiment, for example, the control unit (described further below) may output a PWM control signal to the motor 65 based on the input from the sensor 110 in order to control the motor 65.

[0027] The handle 6 may include a middle handle piece 104 adjacent to the upper portion of the firing trigger 20. The handle 6 also may comprise a bias spring 112 connected between posts on the middle handle piece 104 and the firing trigger 20. The bias spring 112 may bias the firing trigger 20 to its fully open position. In that way, when the operator releases the firing trigger 20, the bias spring 112 will pull the firing trigger 20 to its open position, thereby removing actuation of the sensor 110, thereby stopping rotation of the motor 65. Moreover, by virtue of the bias spring 112, any time a user closes the firing trigger 20, the user will experience resistance to the closing operation, thereby providing the user with feedback as to the amount of rotation exerted by the motor 65. Further, the operator could stop retracting the firing trig-

ger 20 to thereby remove force from the sensor 100, to thereby stop the motor 65. As such, the user may stop the deployment of the end effector 12, thereby providing a measure of control of the cutting/fastening operation to the operator.

[0028] The distal end of the helical gear drum 80 includes a distal drive shaft 120 that drives a ring gear 122, which mates with a pinion gear 124. The pinion gear 124 is connected to the main drive shaft 48 of the main drive shaft assembly. In that way, rotation of the motor 65 causes the main drive shaft assembly to rotate, which causes actuation of the end effector 12, as described above.

[0029] The ring 84 threaded on the helical gear drum 80 may include a post 86 that is disposed within a slot 88 of a slotted arm 90. The slotted arm 90 has an opening 92 at its opposite end 94 that receives a pivot pin 96 that is connected between the handle exterior side pieces 59, 60. The pivot pin 96 is also disposed through an opening 100 in the firing trigger 20 and an opening 102 in the middle handle piece 104.

[0030] In addition, the handle 6 may include a reverse motor (or end-of-stroke sensor) 130 and a stop motor (or beginning-of-stroke) sensor 142. In various embodiments, the reverse motor sensor 130 may be a limit switch located at the distal end of the helical gear drum 80 such that the ring 84 threaded on the helical gear drum 80 contacts and trips the reverse motor sensor 130 when the ring 84 reaches the distal end of the helical gear drum 80. The reverse motor sensor 130, when activated, sends a signal to the control unit which sends a signal to the motor 65 to reverse its rotation direction, thereby withdrawing the knife 32 of the end effector 12 following the cutting operation.

[0031] The stop motor sensor 142 may be, for example, a normally-closed limit switch. In various embodiments, it may be located at the proximate end of the helical gear drum 80 so that the ring 84 trips the switch 142 when the ring 84 reaches the proximate end of the helical gear drum 80.

[0032] In operation, when an operator of the instrument 10 pulls back the firing trigger 20, the sensor 110 detects the deployment of the firing trigger 20 and sends a signal to the control unit which sends a signal to the motor 65 to cause forward rotation of the motor 65 at, for example, a rate proportional to how hard the operator pulls back the firing trigger 20. The forward rotation of the motor 65 in turn causes the ring gear 78 at the distal end of the planetary gear assembly 72 to rotate, thereby causing the helical gear drum 80 to rotate, causing the ring 84 threaded on the helical gear drum 80 to travel distally along the helical gear drum 80. The rotation of the helical gear drum 80 also drives the main drive shaft assembly as described above, which in turn causes deployment of the knife 32 in the end effector 12. That is, the knife 32 and sled 33 are caused to traverse the channel 22 longitudinally, thereby cutting tissue clamped in the end effector 12. Also, the stapling operation of the end effector 12 is caused to happen in embodiments where a stapling-

type end effector is used.

[0033] By the time the cutting/stapling operation of the end effector 12 is complete, the ring 84 on the helical gear drum 80 will have reached the distal end of the helical gear drum 80, thereby causing the reverse motor sensor 130 to be tripped, which sends a signal to the control unit which sends a signal to the motor 65 to cause the motor 65 to reverse its rotation. This in turn causes the knife 32 to retract, and also causes the ring 84 on the helical gear drum 80 to move back to the proximate end of the helical gear drum 80.

[0034] The middle handle piece 104 includes a backside shoulder 106 that engages the slotted arm 90 as best shown in Figures 8 and 9. The middle handle piece 104 also has a forward motion stop 107 that engages the firing trigger 20. The movement of the slotted arm 90 is controlled, as explained above, by rotation of the motor 65. When the slotted arm 90 rotates CCW as the ring 84 travels from the proximate end of the helical gear drum 80 to the distal end, the middle handle piece 104 will be free to rotate CCW. Thus, as the user draws in the firing trigger 20, the firing trigger 20 will engage the forward motion stop 107 of the middle handle piece 104, causing the middle handle piece 104 to rotate CCW. Due to the backside shoulder 106 engaging the slotted arm 90, however, the middle handle piece 104 will only be able to rotate CCW as far as the slotted arm 90 permits. In that way, if the motor 65 should stop rotating for some reason, the slotted arm 90 will stop rotating, and the user will not be able to further draw in the firing trigger 20 because the middle handle piece 104 will not be free to rotate CCW due to the slotted arm 90.

[0035] Components of an exemplary closure system for closing (or clamping) the anvil 24 of the end effector 12 by retracting the closure trigger 18 are also shown in Figures 7-10. In the illustrated embodiment, the closure system includes a yoke 250 connected to the closure trigger 18 by a pin 251 that is inserted through aligned openings in both the closure trigger 18 and the yoke 250. A pivot pin 252, about which the closure trigger 18 pivots, is inserted through another opening in the closure trigger 18 which is offset from where the pin 251 is inserted through the closure trigger 18. Thus, retraction of the closure trigger 18 causes the upper part of the closure trigger 18, to which the yoke 250 is attached via the pin 251, to rotate CCW. The distal end of the yoke 250 is connected, via a pin 254, to a first closure bracket 256. The first closure bracket 256 connects to a second closure bracket 258. Collectively, the closure brackets 256, 258 define an opening in which the proximate end of the proximate closure tube 40 (see Figure 4) is seated and held such that longitudinal movement of the closure brackets 256, 258 causes longitudinal motion by the proximate closure tube 40. The instrument 10 also includes a closure rod 260 disposed inside the proximate closure tube 40. The closure rod 260 may include a window 261 into which a post 263 on one of the handle exterior pieces, such as exterior lower side piece 59 in the

illustrated embodiment, is disposed to fixedly connect the closure rod 260 to the handle 6. In that way, the proximate closure tube 40 is capable of moving longitudinally relative to the closure rod 260. The closure rod 260 may also include a distal collar 267 that fits into a cavity 269 in proximate spine tube 46 and is retained therein by a cap 271 (see Figure 4).

[0036] In operation, when the yoke 250 rotates due to retraction of the closure trigger 18, the closure brackets 256, 258 cause the proximate closure tube 40 to move distally (i.e., away from the handle end of the instrument 10), which causes the distal closure tube 42 to move distally, which causes the anvil 24 to rotate about the pivot point 25 into the clamped or closed position. When the closure trigger 18 is unlocked from the locked position, the proximate closure tube 40 is caused to slide proximally, which causes the distal closure tube 42 to slide proximally, which, by virtue of the tab 27 being inserted in the window 45 of the distal closure tube 42, causes the anvil 24 to pivot about the pivot point 25 into the open or unclamped position. In that way, by retracting and locking the closure trigger 18, an operator may clamp tissue between the anvil 24 and channel 22, and may unclamp the tissue following the cutting/stapling operation by unlocking the closure trigger 18 from the locked position.

[0037] The control unit (described further below) may receive the outputs from end-of-stroke and beginning-of-stroke sensors 130, 142 and the run-motor sensor 110, and may control the motor 65 based on the inputs. For example, when an operator initially pulls the firing trigger 20 after locking the closure trigger 18, the run-motor sensor 110 is actuated. If the staple cartridge 34 is present in the end effector 12, a cartridge lockout sensor (not shown) may be closed, in which case the control unit may output a control signal to the motor 65 to cause the motor 65 to rotate in the forward direction. When the end effector 12 reaches the end of its stroke, the reverse motor sensor 130 will be activated. The control unit may receive this output from the reverse motor sensor 130 and cause the motor 65 to reverse its rotational direction. When the knife 32 is fully retracted, the stop motor sensor switch 142 is activated, causing the control unit to stop the motor 65.

[0038] In other embodiments, rather than a proportional-type sensor 110, an on-off type sensor could be used. In such embodiments, the rate of rotation of the motor 65 would not be proportional to the force applied by the operator. Rather, the motor 65 would generally rotate at a constant rate. But the operator would still experience force feedback because the firing trigger 20 is geared into the gear drive train.

[0039] The instrument 10 may include a number of sensor transponders in the end effector 12 for sensing various conditions related to the end effector 12, such as sensor transponders for determining the status of the staple cartridge 34 (or other type of cartridge depending on the type of surgical instrument), the progress of the sta-

pler during closure and firing, etc. The sensor transponders may be passively powered by inductive signals, as described further below, although in other embodiments the transponders could be powered by a remote power source, such as a battery in the end effector 12, for example. The sensor transponder(s) could include magnetoresistive, optical, electromechanical, RFID, MEMS, motion or pressure sensors, for example. These sensor transponders may be in communication with a control unit 300, which may be housed in the handle 6 of the instrument 10, for example, as shown in Figure 11.

[0040] As shown in Figure 12, according to various embodiments the control unit 300 may comprise a processor 306 and one or more memory units 308. By executing instruction code stored in the memory 308, the processor 306 may control various components of the instrument 10, such as the motor 65 or a user display (not shown), based on inputs received from the various end effector sensor transponders and other sensor(s) (such as the run-motor sensor 110, the end-of-stroke sensor 130, and the beginning-of-stroke sensor 142, for example). The control unit 300 may be powered by the battery 64 during surgical use of instrument 10. The control unit 300 may comprise an inductive element 302 (e.g., a coil or antenna) to pick up wireless signals from the sensor transponders, as described in more detail below. Input signals received by the inductive element 302 acting as a receiving antenna may be demodulated by a demodulator 310 and decoded by a decoder 312. The input signals may comprise data from the sensor transponders in the end effector 12, which the processor 306 may use to control various aspects of the instrument 10.

[0041] To transmit signals to the sensor transponders, the control unit 300 may comprise an encoder 316 for encoding the signals and a modulator 318 for modulating the signals according to the modulation scheme. The inductive element 302 may act as the transmitting antenna. The control unit 300 may communicate with the sensor transponders using any suitable wireless communication protocol and any suitable frequency (e.g., an ISM band). Also, the control unit 300 may transmit signals at a different frequency range than the frequency range of the received signals from the sensor transponders. Also, although only one antenna (inductive element 302) is shown in Figure 12, in other embodiments the control unit 300 may have separate receiving and transmitting antennas.

[0042] According to various embodiments, the control unit 300 may comprise a microcontroller, a microprocessor, a field programmable gate array (FPGA), one or more other types of integrated circuits (e.g., RF receivers and PWM controllers), and/or discrete passive components. The control units may also be embodied as system-on-chip (SoC) or a system-in-package (SIP), for example.

[0043] As shown in Figure 11, the control unit 300 may be housed in the handle 6 of the instrument 10 and one or more of the sensor transponders 368 for the instrument

10 may be located in the end effector 12. To deliver power and/or transmit data to or from the sensor transponders 368 in the end effector 12, the inductive element 302 of the control unit 300 may be inductively coupled to a secondary inductive element (e.g., a coil) 320 positioned in the shaft 8 distally from the rotation joint 29. The secondary inductive element 320 is preferably electrically insulated from the conductive shaft 8.

[0044] The secondary inductive element 320 may be connected by an electrically conductive, insulated wire 322 to a distal inductive element (e.g., a coil) 324 located near the end effector 12, and preferably distally relative to the articulation pivot 14. The wire 322 may be made of an electrically conductive polymer and/or metal (e.g., copper) and may be sufficiently flexible so that it could pass through the articulation pivot 14 and not be damaged by articulation. The distal inductive element 324 may be inductively coupled to the sensor transponder 368 in, for example, the cartridge 34 of the end effector 12. The transponder 368, as described in more detail below, may include an antenna (or coil) for inductive coupling to the distal coil 324, a sensor and integrated control electronics for receiving and transmitting wireless communication signals.

[0045] The transponder 368 may use a portion of the power of the inductive signal received from the distal inductive element 326 to passively power the transponder 368. Once sufficiently powered by the inductive signals, the transponder 368 may receive and transmit data to the control unit 300 in the handle 6 via (i) the inductive coupling between the transponder 368 and the distal inductive element 324, (ii) the wire 322, and (iii) the inductive coupling between the secondary inductive element 320 and the control unit 300. That way, the control unit 300 may communicate with the transponder 368 in the end effector 12 without a direct wired connection through complex mechanical joints like the rotating joint 29 and/or without a direct wired connection from the shaft 8 to the end effector 12, places where it may be difficult to maintain such a wired connection. In addition, because the distances between the inductive elements (e.g., the spacing between (i) the transponder 368 and the distal inductive element 324, and (ii) the secondary inductive element 320 and the control unit 300) and fixed and known, the couplings could be optimized for inductive transfer of energy. Also, the distances could be relatively short so that relatively low power signals could be used to thereby minimize interference with other systems in the use environment of the instrument 10.

[0046] In the embodiment of Figure 12, the inductive element 302 of the control unit 300 is located relatively near to the control unit 300. According to other embodiments, as shown in Figure 13, the inductive element 302 of the control unit 300 may be positioned closer to the rotating joint 29 so that it is closer to the secondary inductive element 320, thereby reducing the distance of the inductive coupling in such an embodiment. Alternatively, the control unit 300 (and hence the inductive ele-

ment 302) could be positioned closer to the secondary inductive element 320 to reduce the spacing.

[0047] In other embodiments, more or fewer than two inductive couplings may be used. For example, in some embodiments, the surgical instrument 10 may use a single inductive coupling between the control unit 300 in the handle 6 and the transponder 368 in the end effector 12, thereby eliminating the inductive elements 320, 324 and the wire 322. Of course, in such an embodiment, a stronger signal may be required due to the greater distance between the control unit 300 in the handle 6 and the transponder 368 in the end effector 12. Also, more than two inductive couplings could be used. For example, if the surgical instrument 10 had numerous complex mechanical joints where it would be difficult to maintain a direct wired connection, inductive couplings could be used to span each such joint. For example, inductive couplers could be used on both sides of the rotary joint 29 and both sides of the articulation pivot 14, with the inductive element 321 on the distal side of the rotary joint 29 connected by a wire 322 to the inductive element 324 of the proximate side of the articulation pivot, and a wire 323 connecting the inductive elements 325, 326 on the distal side of the articulation pivot 14 as shown in Figure 14. In this embodiment, the inductive element 326 may communicate with the sensor transponder 368.

[0048] In addition, the transponder 368 may include a number of different sensors. For example, it may include an array of sensors. Further, the end effector 12 could include a number of sensor transponders 368 in communication with the distal inductive element 324 (and hence the control unit 300). Also, the inductive elements 320, 324 may or may not include ferrite cores. As mentioned before, they are also preferably insulated from the electrically conductive outer shaft (or frame) of the instrument 10 (e.g., the closure tubes 40, 42), and the wire 322 is also preferably insulated from the outer shaft 8.

[0049] Figure 15 is a diagram of an end effector 12 including a transponder 368 held or embedded in the cartridge 34 at the distal end of the channel 22. The transponder 368 may be connected to the cartridge 34 by a suitable bonding material, such as epoxy. In this embodiment, the transponder 368 includes a magnetoresistive sensor. The anvil 24 also includes a permanent magnet 369 at its distal end and generally facing the transponder 368. The end effector 12 also includes a permanent magnet 370 connected to the sled 33 in this example embodiment. This allows the transponder 368 to detect both opening/closing of the end effector 12 (due to the permanent magnet 369 moving further or closer to the transponder as the anvil 24 opens and closes) and completion of the stapling/cutting operation (due to the permanent magnet 370 moving toward the transponder 368 as the sled 33 traverses the channel 22 as part of the cutting operation).

[0050] Figure 15 also shows the staples 380 and the staple drivers 382 of the staple cartridge 34. As explained previously, according to various embodiments, when the

sled 33 traverses the channel 22, the sled 33 drives the staple drivers 382 which drive the staples 380 into the severed tissue held in the end effector 12, the staples 380 being formed against the anvil 24. As noted above, such a surgical cutting and fastening instrument is but one type of surgical instrument in which the present invention may be advantageously employed. Various embodiments of the present invention may be used in any type of surgical instrument having one or more sensor transponders.

[0051] In the embodiments described above, the battery 64 powers (at least partially) the firing operation of the instrument 10. As such, the instrument may be a so-called "power-assist" device. More details and additional embodiments of power-assist devices are described in the '573 application, which is incorporated herein. It should be recognized, however, that the instrument 10 need not be a power-assist device and that this is merely an example of a type of device that may utilize aspects of the present invention. For example, the instrument 10 may include a user display (such as a LCD or LED display) that is powered by the battery 64 and controlled by the control unit 300. Data from the sensor transponders 368 in the end effector 12 may be displayed on such a display.

[0052] In another embodiment, the shaft 8 of the instrument 10, including for example, the proximate closure tube 40 and the distal closure tube 42, may collectively serve as part of an antenna for the control unit 300 by radiating signals to the sensor transponder 368 and receiving radiated signals from the sensor transponder 368. That way, signals to and from the remote sensor in the end effector 12 may be transmitted via the shaft 8 of the instrument 10.

[0053] The proximate closure tube 40 may be grounded at its proximate end by the exterior lower and upper side pieces 59-62, which may be made of a nonelectrically conductive material, such as plastic. The drive shaft assembly components (including the main drive shaft 48 and secondary drive shaft 50) inside the proximate and distal closure tubes 40, 42 may also be made of a nonelectrically conductive material, such as plastic. Further, components of end effector 12 (such as the anvil 24 and the channel 22) may be electrically coupled to (or in direct or indirect electrical contact with) the distal closure tube 42 such that they may also serve as part of the antenna. Further, the sensor transponder 368 could be positioned such that it is electrically insulated from the components of the shaft 8 and end effector 12 serving as the antenna. For example, the sensor transponder 368 may be positioned in the cartridge 34, which may be made of a nonelectrically conductive material, such as plastic. Because the distal end of the shaft 8 (such as the distal end of the distal closure tube 42) and the portions of the end effector 12 serving as the antenna may be relatively close in distance to the sensor 368, the power for the transmitted signals may be held at low levels, thereby minimizing or reducing interference with other systems in the use en-

vironment of the instrument 10.

[0054] In such an embodiment, as shown in Figure 16, the control unit 300 may be electrically coupled to the shaft 8 of the instrument 10, such as to the proximate closure tube 40, by a conductive link 400 (e.g., a wire). Portions of the outer shaft 8, such as the closure tubes 40, 42, may therefore act as part of an antenna for the control unit 300 by radiating signals to the sensor 368 and receiving radiated signals from the sensor 368. Input signals received by the control unit 300 may be demodulated by the demodulator 310 and decoded by the decoder 312 (see Figure 12). The input signals may comprise data from the sensors 368 in the end effector 12, which the processor 306 may use to control various aspects of the instrument 10, such as the motor 65 or a user display.

[0055] To transmit data signals to or from the sensors 368 in the end effector 12, the link 400 may connect the control unit 300 to components of the shaft 8 of the instrument 10, such as the proximate closure tube 40, which may be electrically connected to the distal closure tube 42. The distal closure tube 42 is preferably electrically insulated from the remote sensor 368, which may be positioned in the plastic cartridge 34 (see Figure 3). As mentioned before, components of the end effector 12, such as the channel 22 and the anvil 24 (see Figure 3), may be conductive and in electrical contact with the distal closure tube 42 such that they, too, may serve as part of the antenna.

[0056] With the shaft 8 acting as the antenna for the control unit 300, the control unit 300 can communicate with the sensor 368 in the end effector 12 without a direct wired connection. In addition, because the distances between shaft 8 and the remote sensor 368 is fixed and known, the power levels could be optimized for low levels to thereby minimize interference with other systems in the use environment of the instrument 10. The sensor 368 may include communication circuitry for radiating signals to the control unit 300 and for receiving signals from the control unit 300, as described above. The communication circuitry may be integrated with the sensor 368.

[0057] In another embodiment, the components of the shaft 8 and/or the end effector 12 may serve as an antenna for the remote sensor 368. In such an embodiment, the remote sensor 368 is electrically connected to the shaft (such as to distal closure tube 42, which may be electrically connected to the proximate closure tube 40) and the control unit 300 is insulated from the shaft 8. For example, the sensor 368 could be connected to a conductive component of the end effector 12 (such as the channel 22), which in turn may be connected to conductive components of the shaft (e.g., the closure tubes 40, 42). Alternatively, the end effector 12 may include a wire (not shown) that connects the remote sensor 368 the distal closure tube 42.

[0058] Typically, surgical instruments, such as the instrument 10, are cleaned and sterilized prior to use. In

one sterilization technique, the instrument 10 is placed in a closed and sealed container 280, such as a plastic or TYVEK container or bag, as shown in Figs. 17 and 18. The container and the instrument are then placed in a field of radiation that can penetrate the container, such as gamma radiation, x-rays, or high-energy electrons. The radiation kills bacteria on the instrument 10 and in the container 280. The sterilized instrument 10 can then be stored in the sterile container 280. The sealed, sterile container 280 keeps the instrument 10 sterile until it is opened in a medical facility or some other use environment. Instead of radiation, other means of sterilizing the instrument 10 may be used, such as ethylene oxide or steam.

[0059] When radiation, such as gamma radiation, is used to sterilize the instrument 10, components of the control unit 300, particularly the memory 308 and the processor 306, may be damaged and become unstable. Thus, according to various embodiments of the present invention, the control unit 300 may be programmed after packaging and sterilization of the instrument 10.

[0060] As shown in Figure 17, a remote programming device 320, which may be a handheld device, may be brought into wireless communication with the control unit 300. The remote programming device 320 may emit wireless signals that are received by the control unit 300 to program the control unit 300 and to power the control unit 300 during the programming operation. That way, the battery 64 does not need to power the control unit 300 during the programming operation. According to various embodiments, the programming code downloaded to the control unit 300 could be of relatively small size, such as 1MB or less, so that a communications protocol with a relatively low data transmission rate could be used if desired. Also, the remote programming unit 320 could be brought into close physical proximity with the surgical instrument 10 so that a low power signal could be used.

[0061] Referring back to Figure 19, the control unit 300 may comprise an inductive coil 402 to pick up wireless signals from a remote programming device 320. A portion of the received signal may be used by a power circuit 404 to power the control unit 300 when it is not being powered by the battery 64.

[0062] Input signals received by the coil 402 acting as a receiving antenna may be demodulated by a demodulator 410 and decoded by a decoder 412. The input signals may comprise programming instructions (e.g., code), which may be stored in a non-volatile memory portion of the memory 308. The processor 306 may execute the code when the instrument 10 is in operation. For example, the code may cause the processor 306 to output control signals to various sub-systems of the instrument 10, such as the motor 65, based on data received from the sensors 368.

[0063] The control unit 300 may also comprise a non-volatile memory unit 414 that comprises boot sequence code for execution by the processor 306. When the control unit 300 receives enough power from the signals from

the remote control unit 320 during the post-sterilization programming operation, the processor 306 may first execute the boot sequence code ("boot loader") 414, which may load the processor 306 with an operating system.

[0064] The control unit 300 may also send signals back to the remote programming unit 320, such as acknowledgement and handshake signals, for example. The control unit 300 may comprise an encoder 416 for encoding the signals to then be sent to the programming device 320 and a modulator 418 for modulating the signals according to the modulation scheme. The coil 402 may act as the transmitting antenna. The control unit 300 and the remote programming device 320 may communicate using any suitable wireless communication protocol (e.g., Bluetooth) and any suitable frequency (e.g., an ISM band). Also, the control unit 300 may transmit signals at a different frequency range than the frequency range of the received signals from the remote programming unit 320.

[0065] Figure 20 is a simplified diagram of the remote programming device 320 according to various embodiments of the present invention. As shown in Figure 20, the remote programming unit 320 may comprise a main control board 230 and a boosted antenna board 232. The main control board 230 may comprise a controller 234, a power module 236, and a memory 238. The memory 238 may store the operating instructions for the controller 234 as well as the programming instructions to be transmitted to the control unit 300 of the surgical instrument 10. The power module 236 may provide a stable DC voltage for the components of the remote programming device 320 from an internal battery (not shown) or an external AC or DC power source (not shown).

[0066] The boosted antenna board 232 may comprise a coupler circuit 240 that is in communication with the controller 234 via an I²C bus, for example. The coupler circuit 240 may communicate with the control unit 300 of the surgical instrument via an antenna 244. The coupler circuit 240 may handle the modulating/demodulating and encoding/decoding operations for transmissions with the control unit. According to other embodiments, the remote programming device 320 could have a discrete modulator, demodulator, encoder and decoder. As shown in Figure 20, the boost antenna board 232 may also comprise a transmitting power amp 246, a matching circuit 248 for the antenna 244, and a filter/amplifier 249 for receiving signals.

[0067] According to other embodiments, as shown in Figure 20, the remote programming device could be in communication with a computer device 460, such as a PC or a laptop, via a USB and/or RS232 interface, for example. In such a configuration, a memory of the computing device 460 may store the programming instructions to be transmitted to the control unit 300. In another embodiment, the computing device 460 could be configured with a wireless transmission system to transmit the programming instructions to the control unit 300.

[0068] In addition, according to other embodiments,

rather than using inductive coupling between the control unit 300 and the remote programming device 320, capacitively coupling could be used. In such an embodiment, the control unit 300 could have a plate instead of a coil, as could the remote programming unit 320.

[0069] In another embodiment, rather than using a wireless communication link between the control unit 300 and the remote programming device 320, the programming device 320 may be physically connected to the control unit 300 while the instrument 10 is in its sterile container 280 in such a way that the instrument 10 remains sterilized. Figure 21 is a diagram of a packaged instrument 10 according to such an embodiment. As shown in Figure 22, the handle 6 of the instrument 10 may include an external connection interface 470. The container 280 may further comprise a connection interface 472 that mates with the external connection interface 470 of the instrument 10 when the instrument 10 is packaged in the container 280. The programming device 320 may include an external connection interface (not shown) that may connect to the connection interface 472 at the exterior of the container 280 to thereby provide a wired connection between the programming device 320 and the external connection interface 470 of the instrument 10.

[0070] The various embodiments of the present invention have been described above in connection with cutting-type surgical instruments. It should be noted, however, that in other embodiments, the inventive surgical instrument disclosed herein need not be a cutting-type surgical instrument, but rather could be used in any type of surgical instrument including remote sensor transponders. For example, it could be a non-cutting endoscopic instrument, a grasper, a stapler, a clip applier, an access device, a drug/gene therapy delivery device, an energy device using ultrasound, RF, laser, etc. In addition, the present invention may be in laparoscopic instruments, for example. The present invention also has application in conventional endoscopic and open surgical instrumentation as well as robotic-assisted surgery.

[0071] The devices disclosed herein can be designed to be disposed of after a single use, or they can be designed to be used multiple times. In either case, however, the device can be reconditioned for reuse after at least one use. Reconditioning can include any combination of the steps of disassembly of the device, followed by cleaning or replacement of particular pieces, and subsequent reassembly. In particular, the device can be disassembled, and any number of the particular pieces or parts of the device can be selectively replaced or removed in any combination. Upon cleaning and/or replacement of particular parts, the device can be reassembled for subsequent use either at a reconditioning facility, or by a surgical team immediately prior to a surgical procedure. Those skilled in the art will appreciate that reconditioning of a device can utilize a variety of techniques for disassembly, cleaning/replacement, and reassembly. Use of such techniques, and the resulting reconditioned device, are all within the scope of the present application.

[0072] Although the present invention has been described herein in connection with certain disclosed embodiments, many modifications and variations to those embodiments may be implemented. For example, different types of end effectors may be employed. Also, where materials are disclosed for certain components, other materials may be used. The foregoing description and following claims are intended to cover all such modification and variations.

[0073] Any patent, publication, or other disclosure material, in whole or in part, that is said to be incorporated by reference herein is incorporated herein only to the extent that the incorporated materials does not conflict with existing definitions, statements, or other disclosure material set forth in this disclosure. As such, and to the extent necessary, the disclosure as explicitly set forth herein supersedes any conflicting material incorporated herein by reference. Any material, or portion thereof, that is said to be incorporated by reference herein, but which conflicts with existing definitions, statements, or other disclosure material set forth herein will only be incorporated to the extent that no conflict arises between that incorporated material and the existing disclosure material.

[0074] The following is a non-exhaustive list of embodiments of the invention that may be claimed in this application:

1. A surgical instrument comprising:

an end effector comprising at least one sensor;
an electrically conductive shaft having a distal end connected to the end effector wherein the sensor is electrically insulated from the shaft;
and
a handle connected to a proximate end of the shaft, the handle housing a control unit, wherein the control unit is electrically coupled to the shaft such that the shaft is configured to radiate signals from the control unit to the sensor and to receive radiated signals from the sensor.

2. The surgical instrument of embodiment 1, wherein the handle further houses:

a motor in communication with the control unit and for powering the end effector; and
a battery for powering the motor.

3. The surgical instrument of embodiment 1, wherein the at least one sensor comprises a magnetoresistive sensor.

4. The surgical instrument of embodiment 1, wherein the at least one sensor comprises a pressure sensor.

5. The surgical instrument of embodiment 1, wherein the at least one sensor comprises a RFID sensor.

6. The surgical instrument of embodiment 1, wherein the at least one sensor comprises a MEMS sensor.

7. The surgical instrument of embodiment 1, wherein the at least one sensor comprises an electromechanical sensor.

8. The surgical instrument of embodiment 1, wherein the at least one sensor is connected to a plastic cartridge of the end effector.

9. The surgical instrument of embodiment 1, wherein the end effector comprises an electrically conductive component coupled to the shaft, wherein the electrically conductive component is configured to radiate data signals to and from the sensor.

10. The surgical instrument of embodiment 1, wherein the surgical instrument comprises an endoscopic surgical instrument.

11. A surgical instrument comprising:

an end effector comprising at least one sensor;
an electrically conductive shaft having a distal end connected to the end effector wherein the sensor is electrically insulated from the shaft;
and
a control unit electrically coupled to the shaft such that the shaft is configured to radiate signals from the control unit to the sensor and to receive radiated signals from the sensor.

12. A surgical instrument comprising:

an end effector comprising at least one sensor;
an electrically conductive shaft having a distal end connected to the end effector, wherein the sensor is electrically coupled to the shaft; and
a control unit electrically insulated from the shaft such that the shaft is configured to radiate signals from the sensor to the control unit and to receive radiated signals from the control unit.

13. A method comprising:

sterilizing the surgical instrument of any preceding embodiment; and
storing the surgical instrument in a sterile container.

Claims

1. A surgical instrument comprising:

an end effector comprising at least one sensor;
and

an electrically conductive shaft having a distal end connected to the end effector wherein the sensor is electrically insulated from the shaft.

2. The surgical instrument of claim 1, further comprising a receiver unit electrically insulated from the shaft configured to receive and send wireless signals from and to the sensor. 5
3. The surgical instrument of claim 1, further comprising a control unit electrically coupled to the shaft such that the shaft is configured to radiate signals from the control unit to the sensor and to receive radiated signals from the sensor. 10
4. The surgical instrument of claim 1, further comprising a control unit electrically insulated from the shaft such that the shaft is configured to radiate signals from the sensor to the control unit and to receive radiated signals from the control unit. 15 20
5. The surgical instrument of claim 1 or 2, further comprising a distal stapling unit for performing at least one surgical task connected to a remotely controllable interface. 25
6. The surgical instrument of claim 1, 2 or 5, further comprising a housing at a proximate end of the shaft, configured to receive at least one of mechanical or electrical inputs. 30
7. The surgical instrument of any preceding claim, wherein the sensor is configured to be passively powered. 35
8. The surgical instrument of claim 3 or 4, further comprising:

a handle connected to a proximate end of the shaft, the handle housing the control unit. 40
9. The surgical instrument of claim 8, wherein the handle further houses:

a motor in communication with the control unit and for powering the end effector; and 45

a battery for powering the motor.
10. The surgical instrument of any preceding claim, wherein the at least one sensor comprises a magnetoresistive sensor, a pressure sensor, a RFID sensor, a MEMS sensor, or an electromechanical sensor. 50
11. The surgical instrument of any preceding claim, wherein the at least one sensor is connected to a plastic cartridge of the end effector. 55

12. The surgical instrument of any preceding claim, wherein the end effector comprises an electrically conductive component coupled to the shaft, wherein the electrically conductive component is configured to radiate data signals to and from the sensor.

13. The surgical instrument of any preceding claim, wherein the surgical instrument comprises an endoscopic surgical instrument.

14. A method comprising:

sterilizing the surgical instrument of any preceding claim; and
storing the surgical instrument in a sterile container.

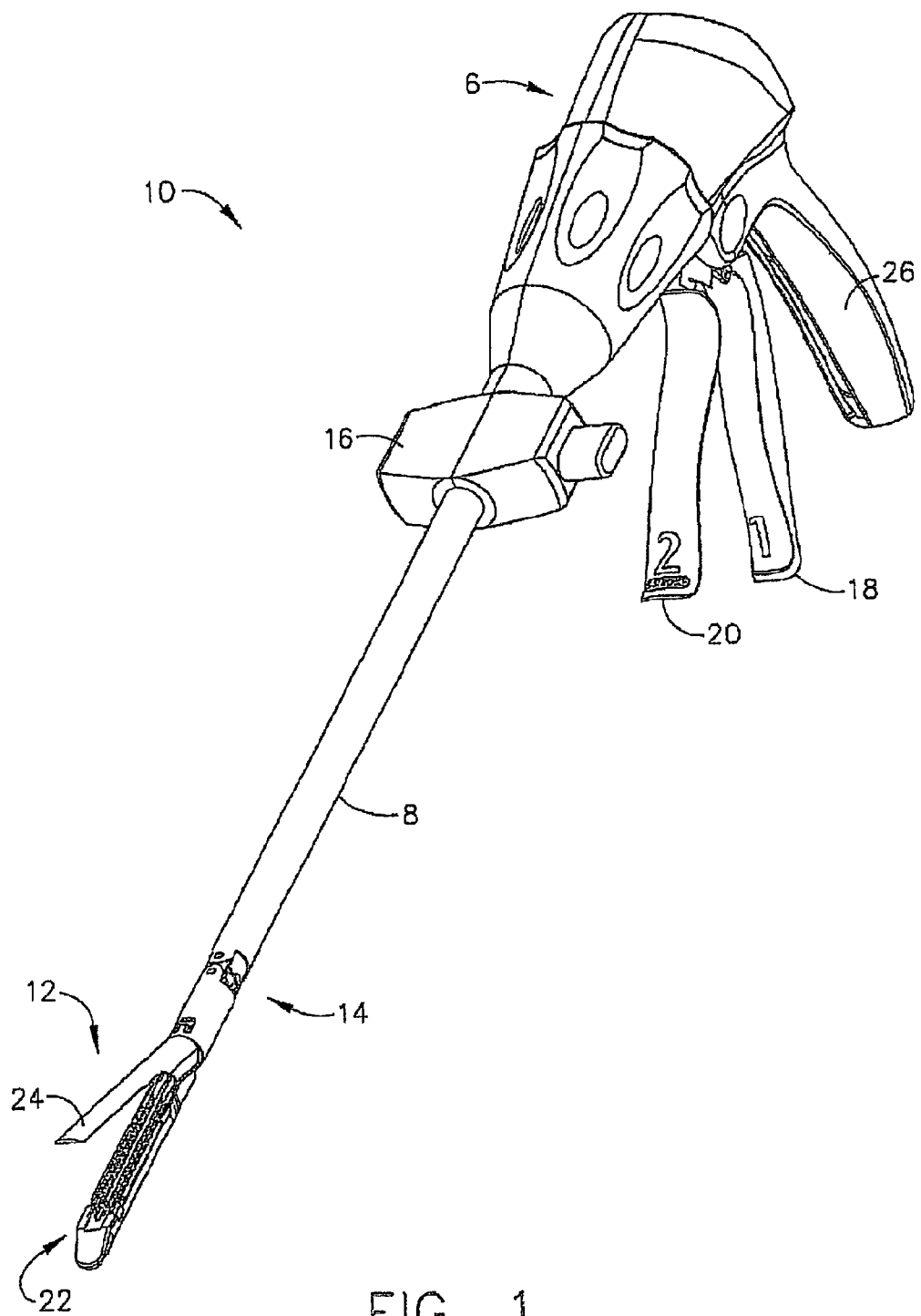


FIG. 1

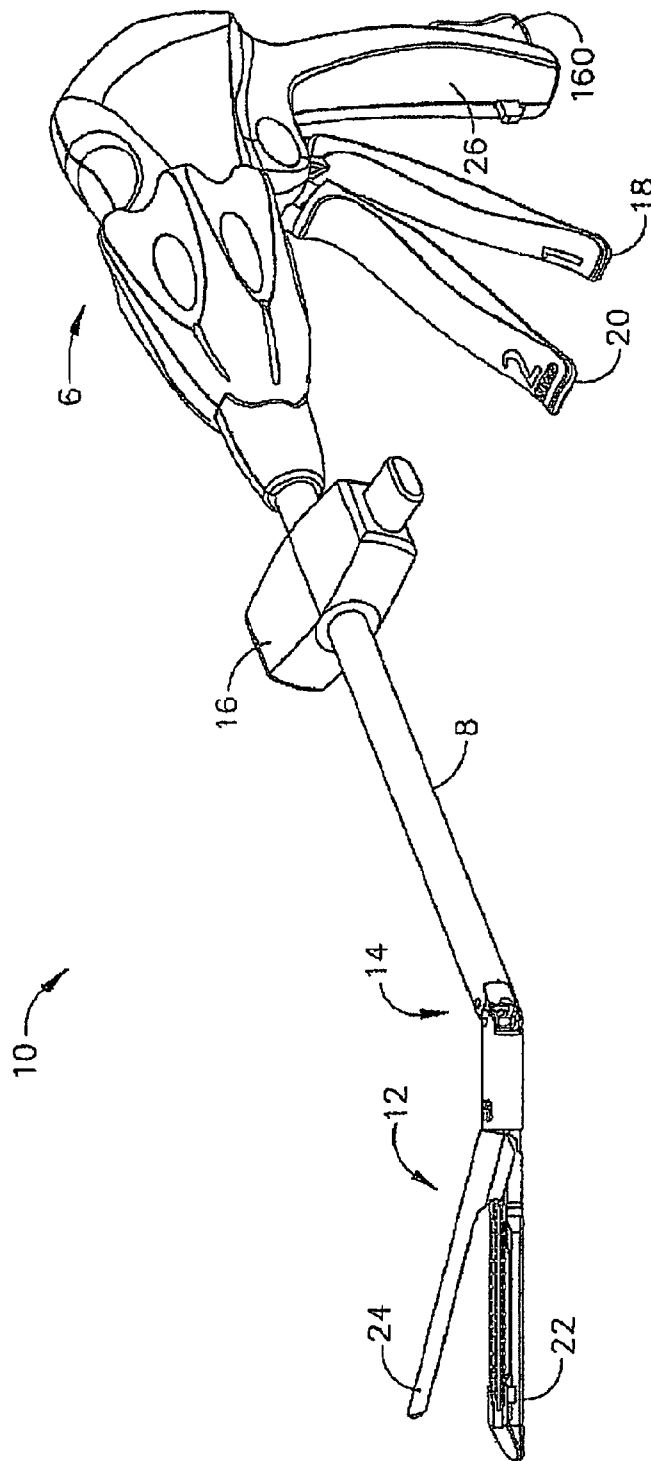


FIG. 2

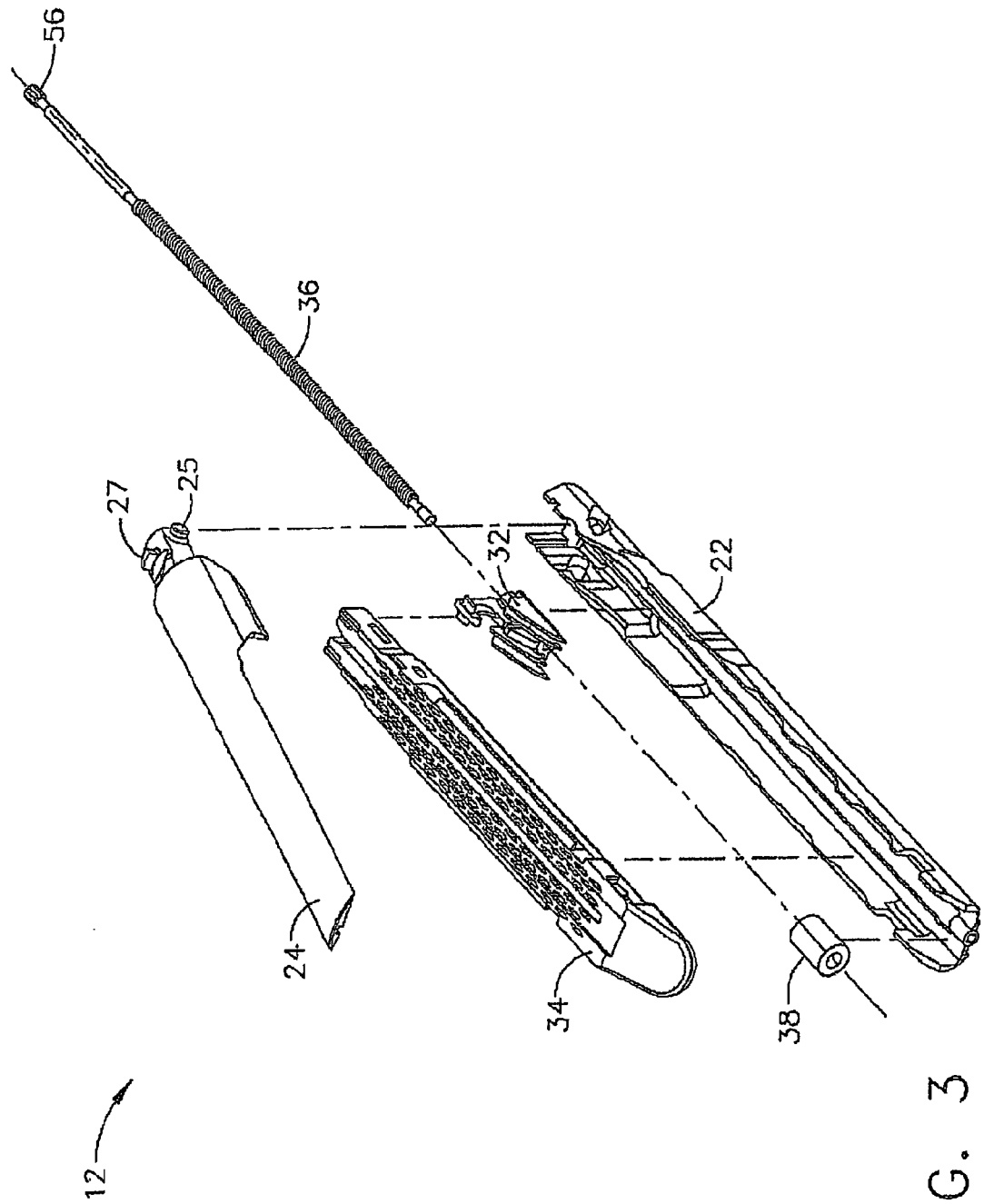


FIG. 3

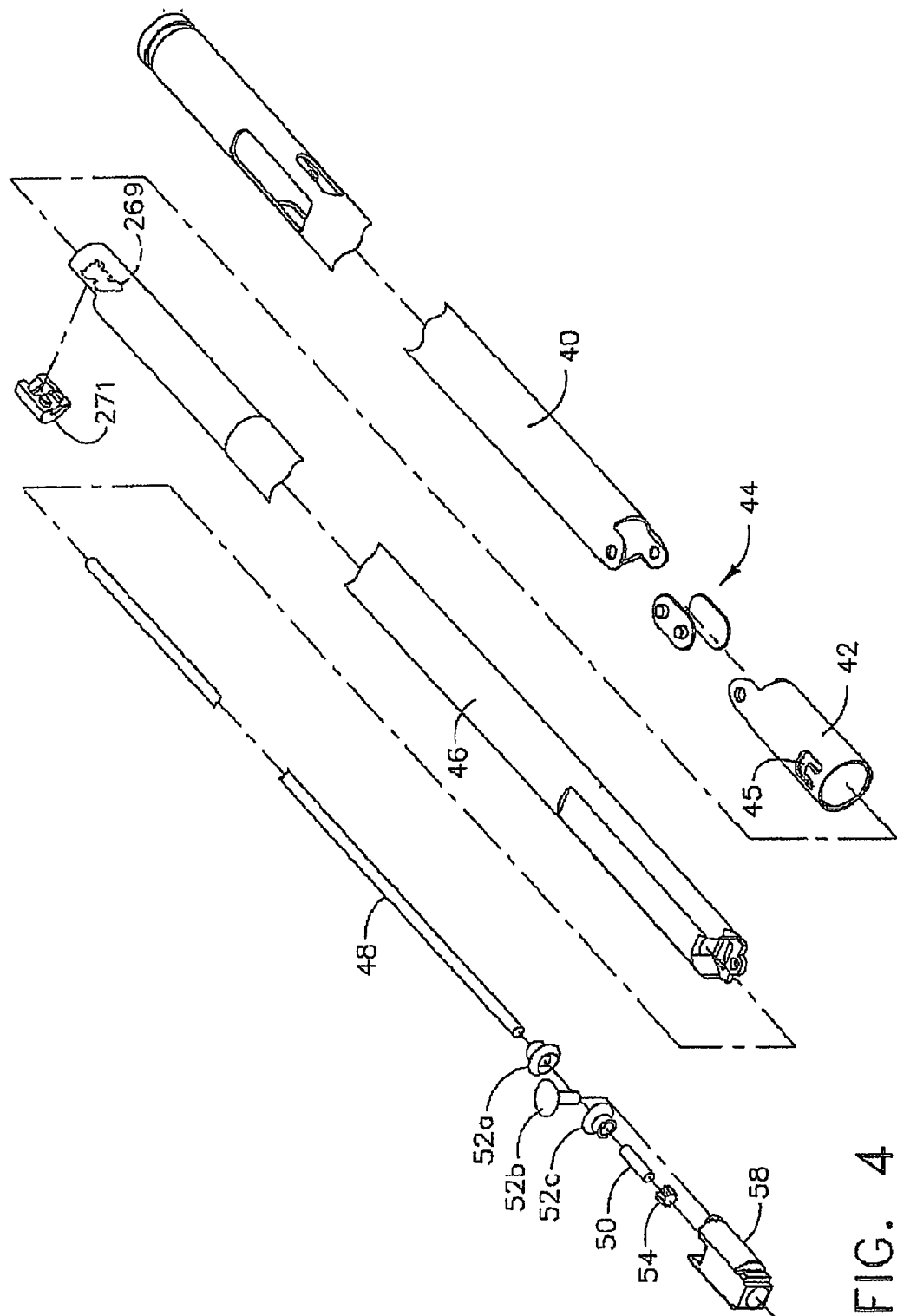


FIG. 4

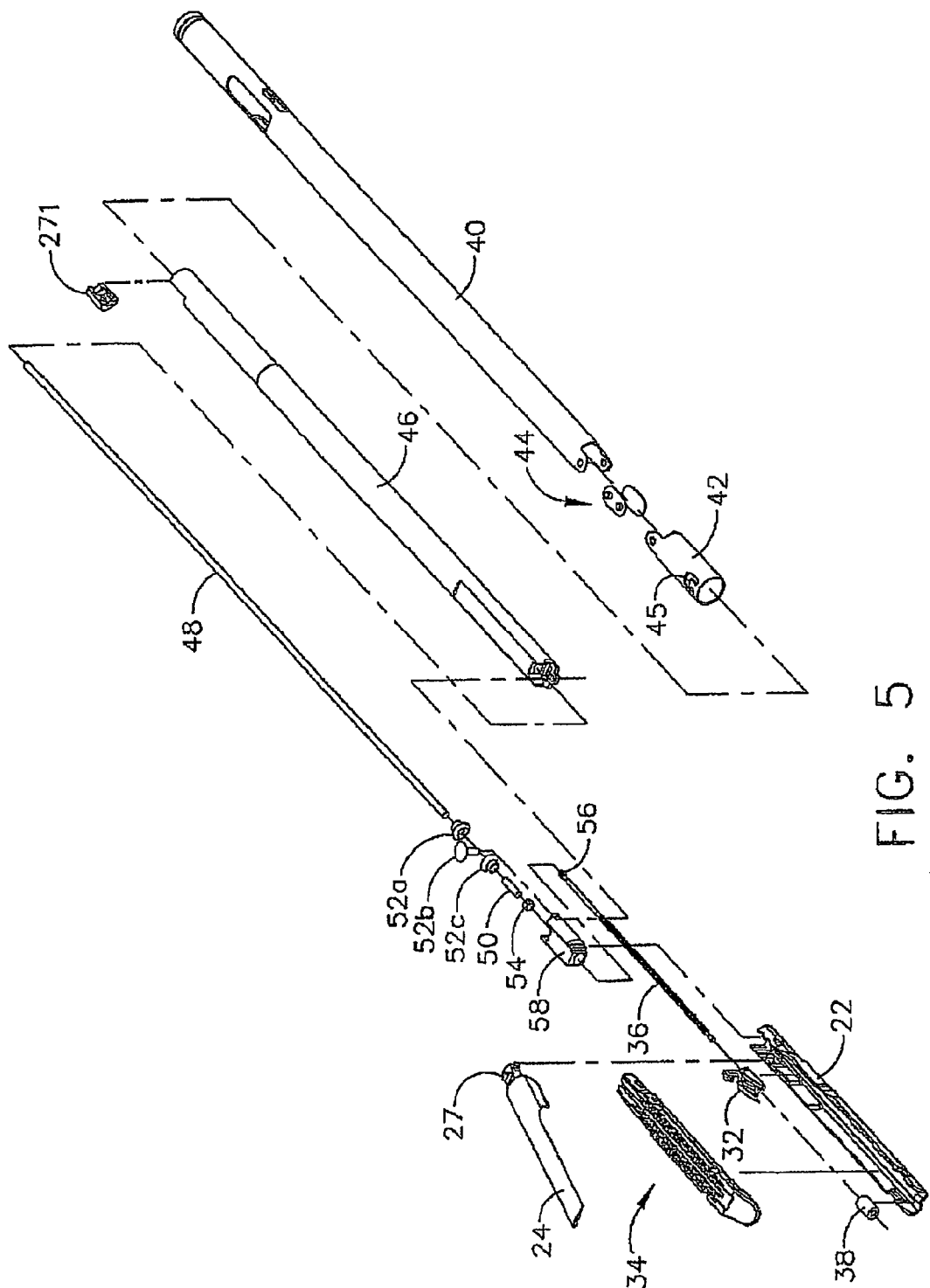


FIG. 5

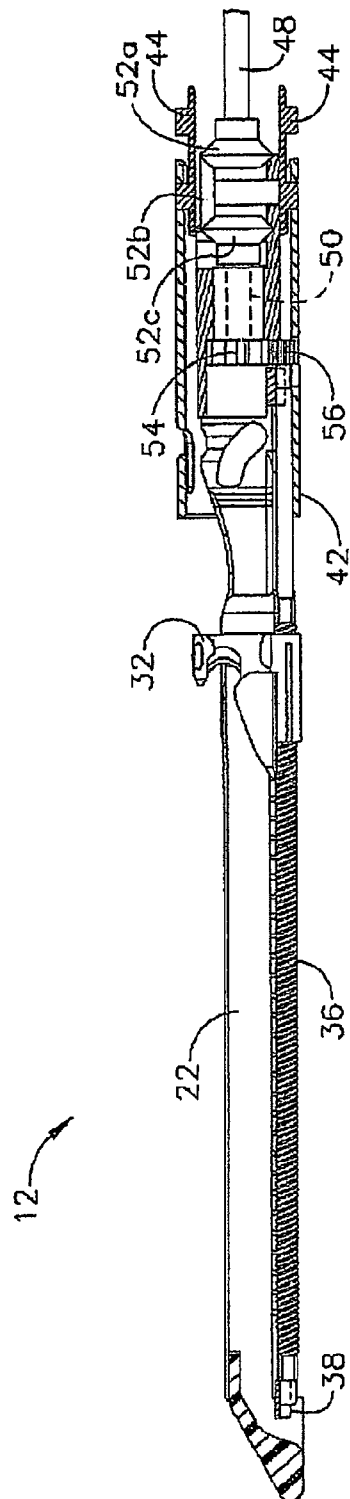
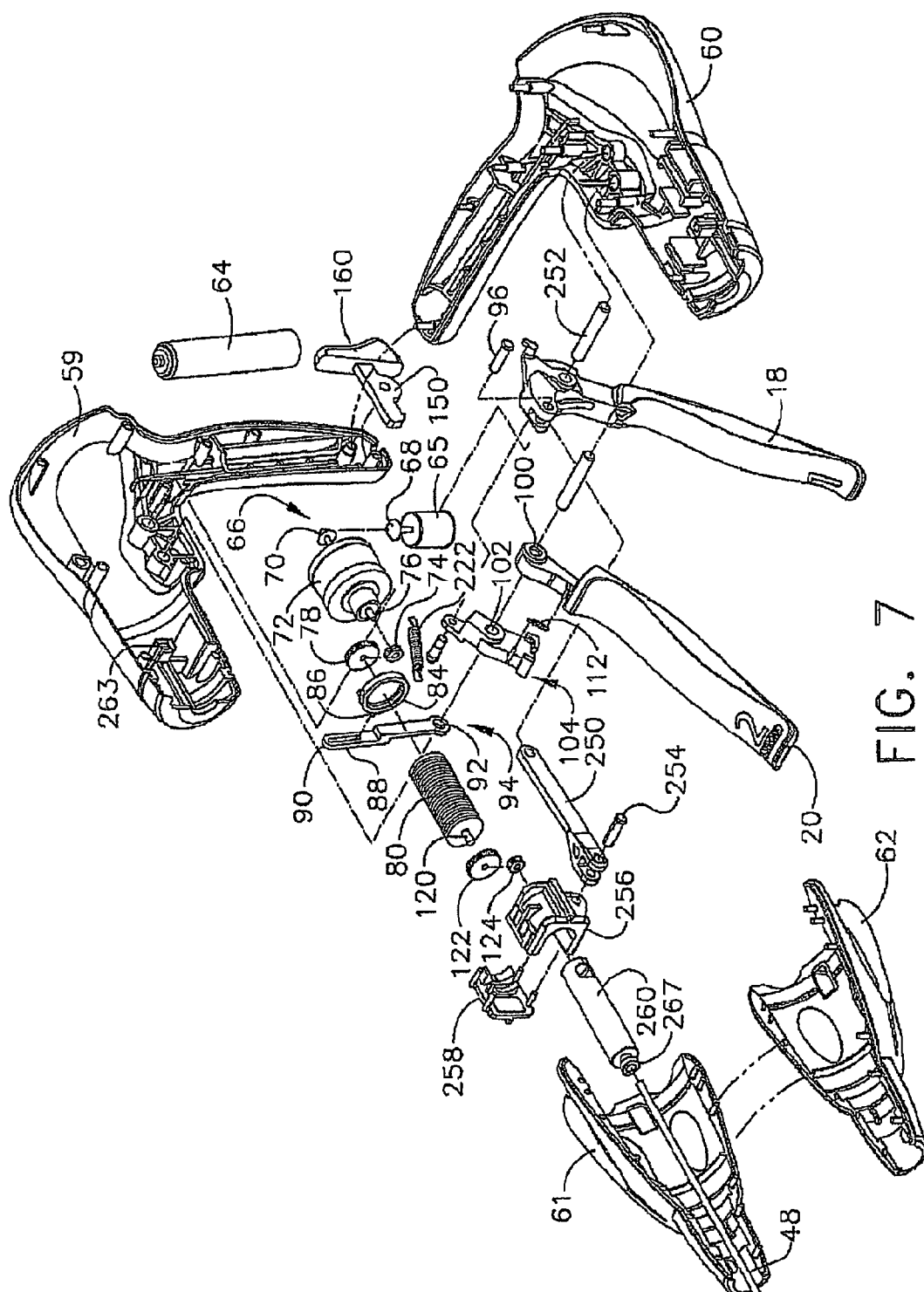


FIG. 6



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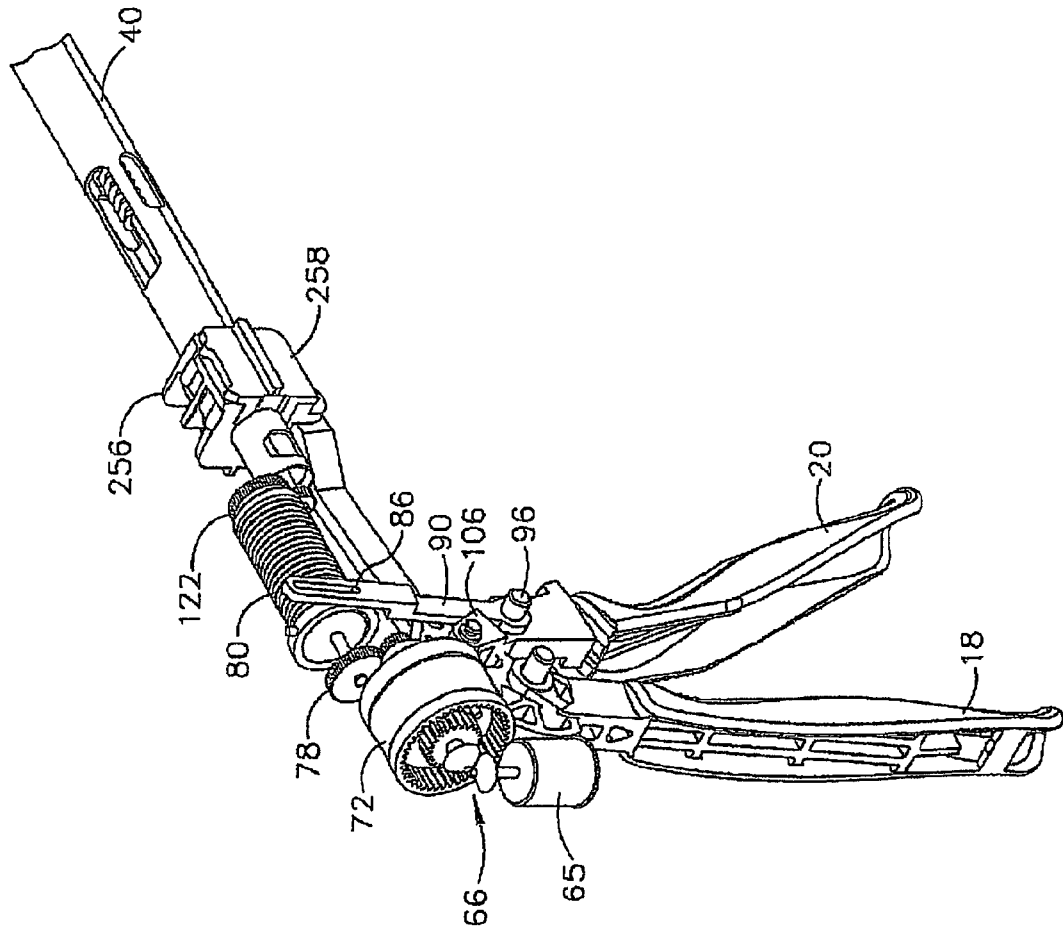


FIG. 8

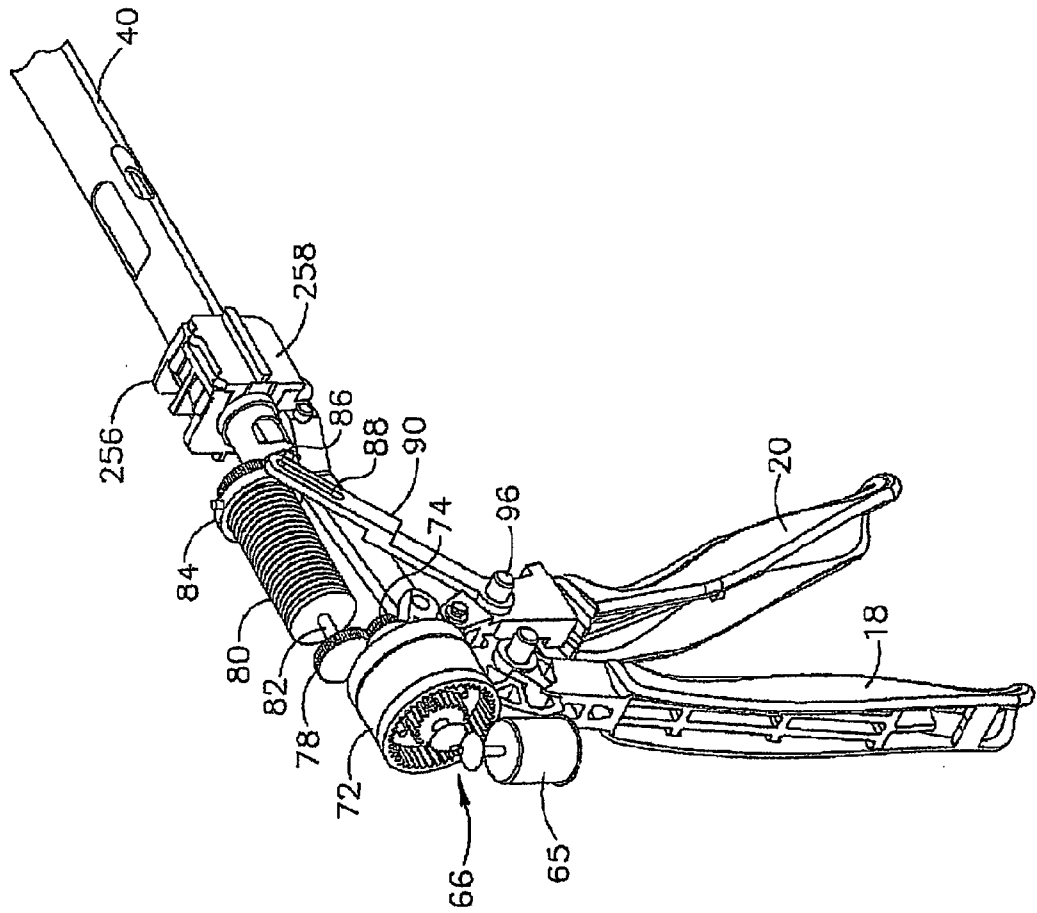


FIG. 9

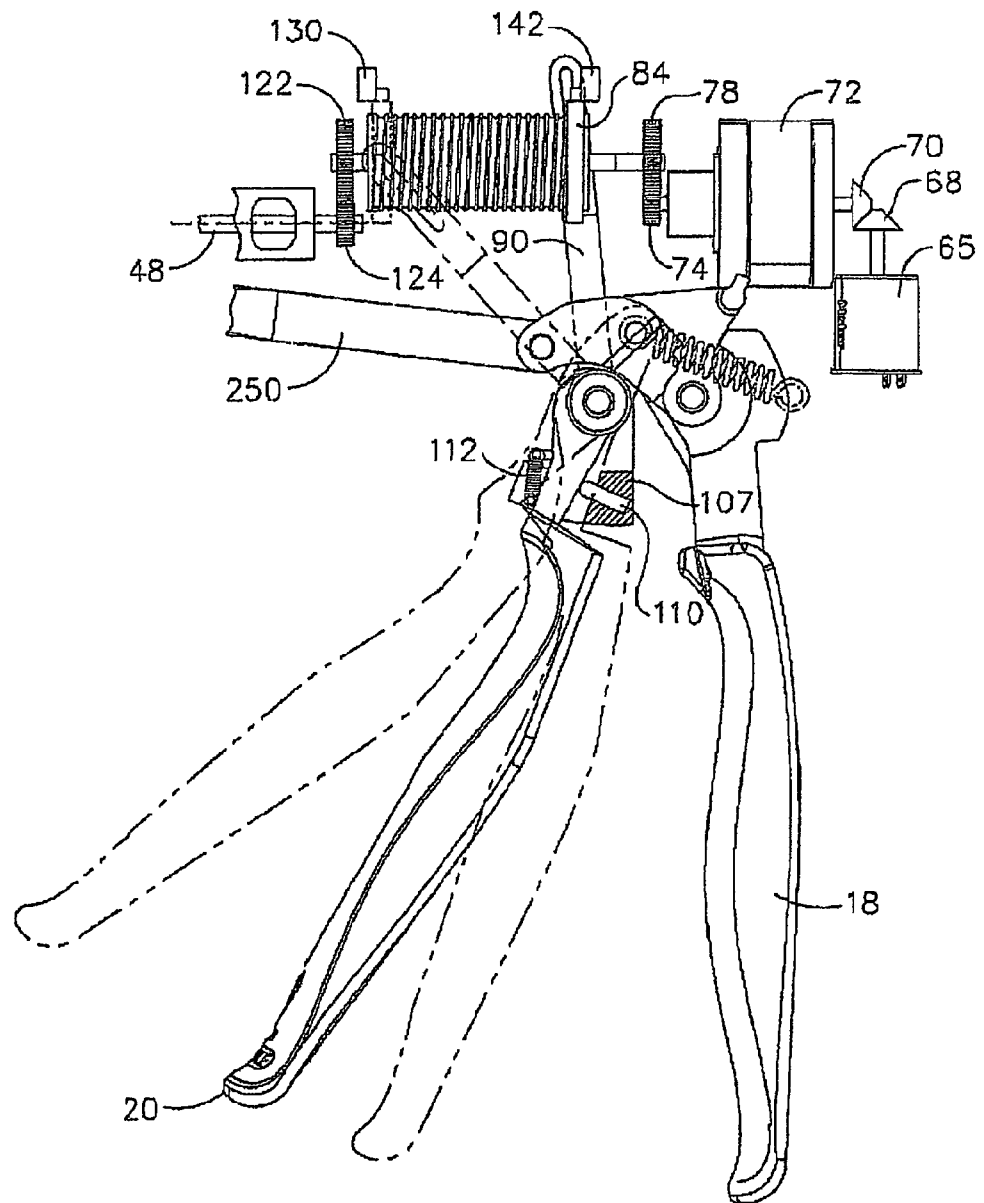


FIG. 10

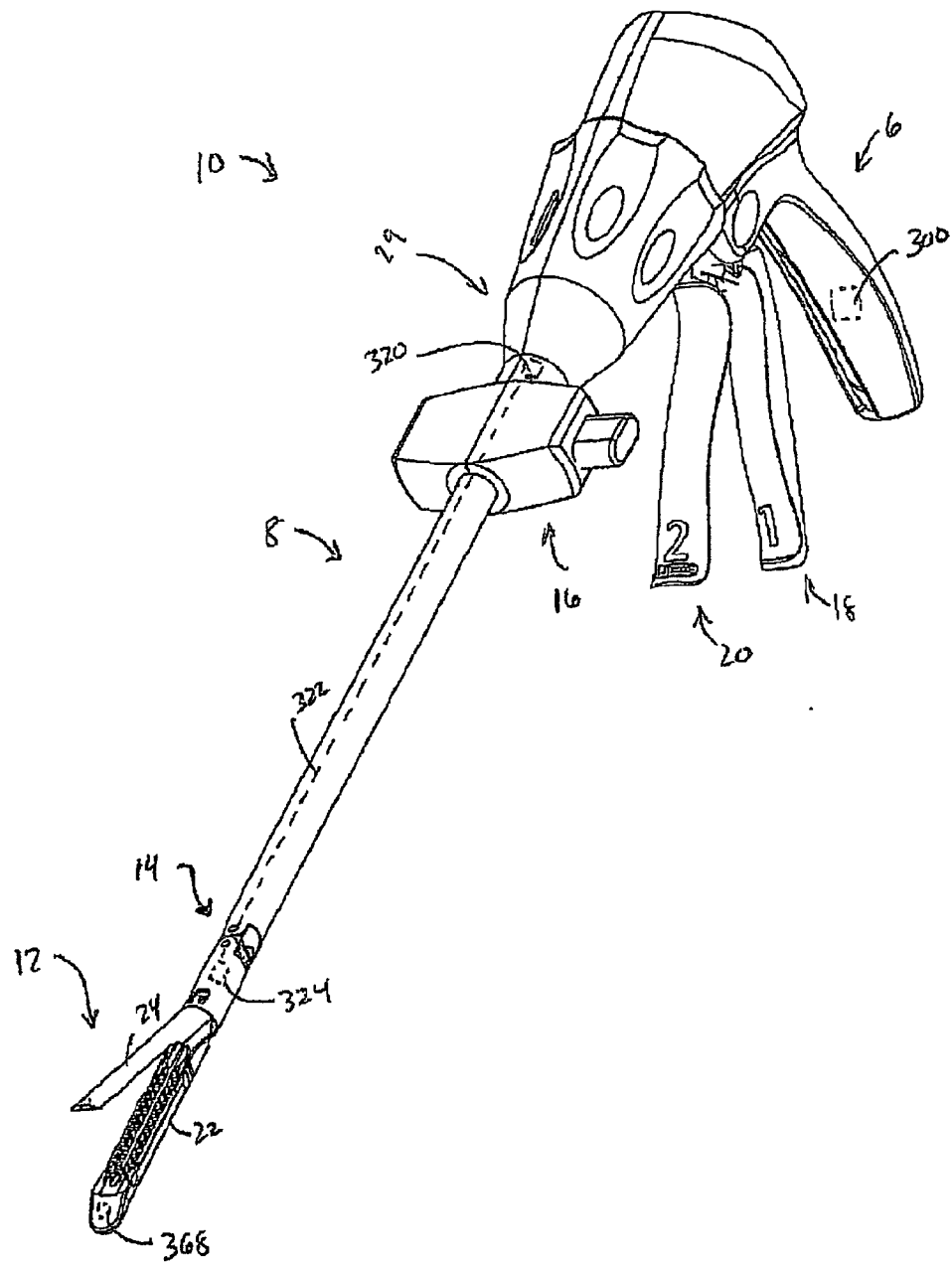
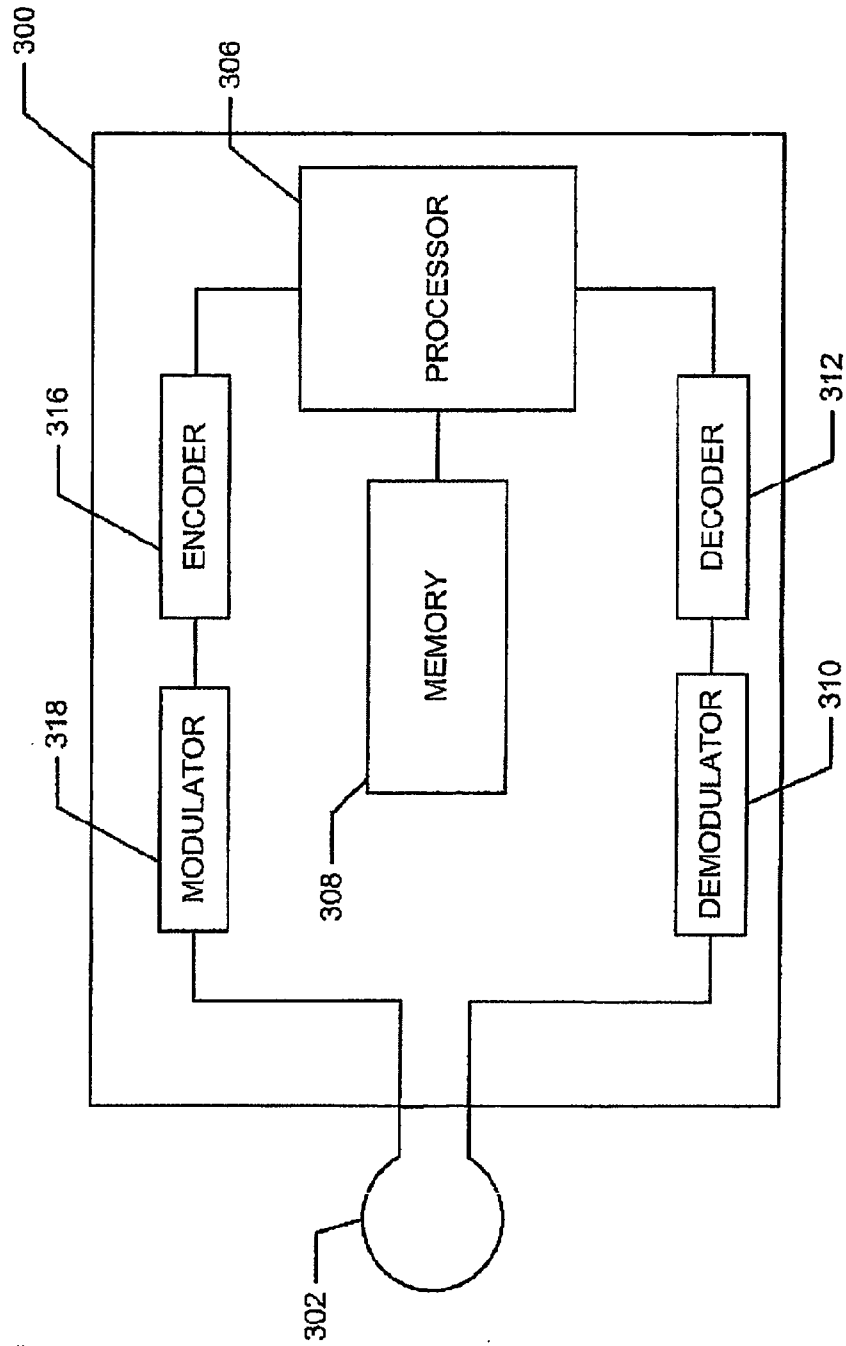


FIG. 11

FIG. 12



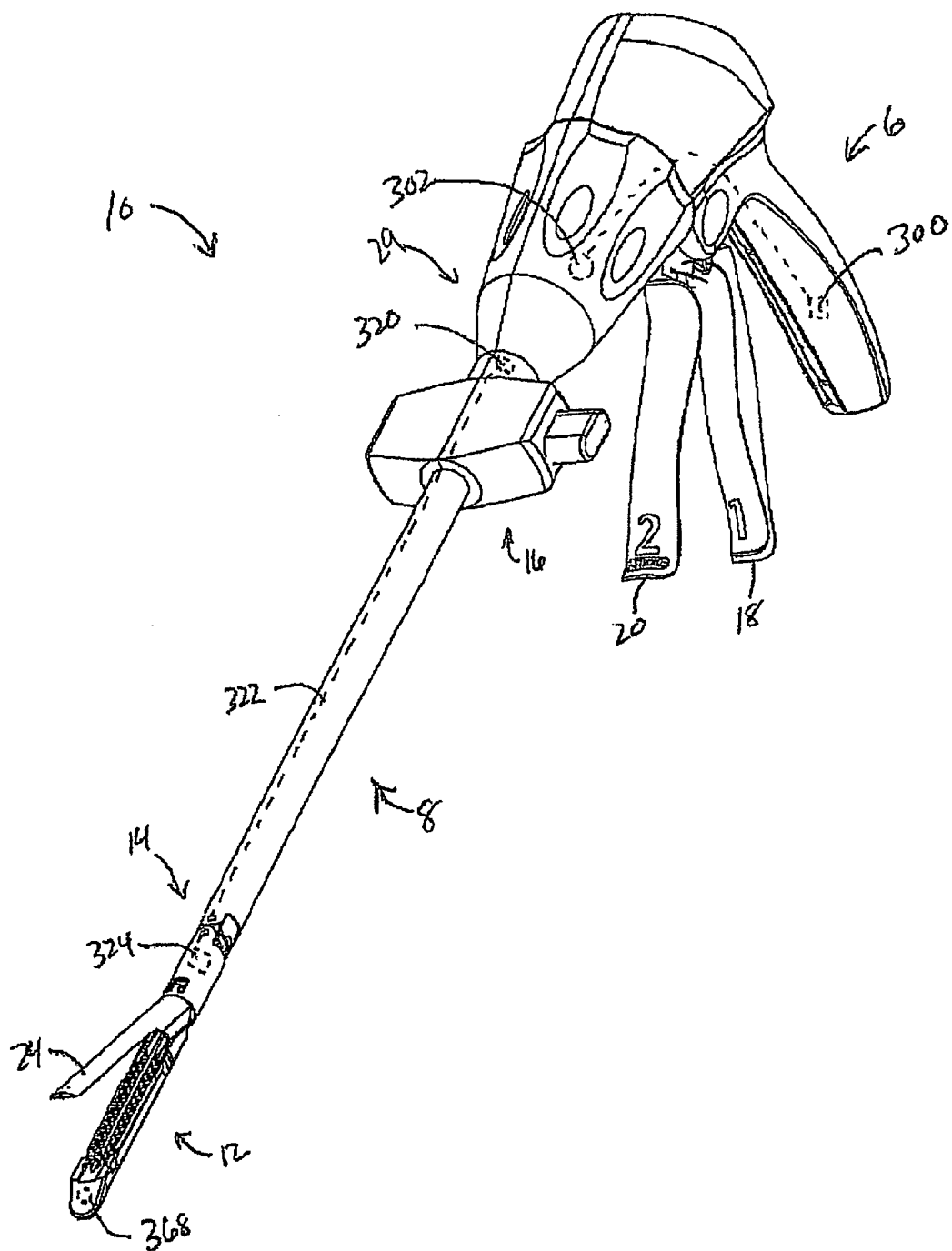


FIG. 13

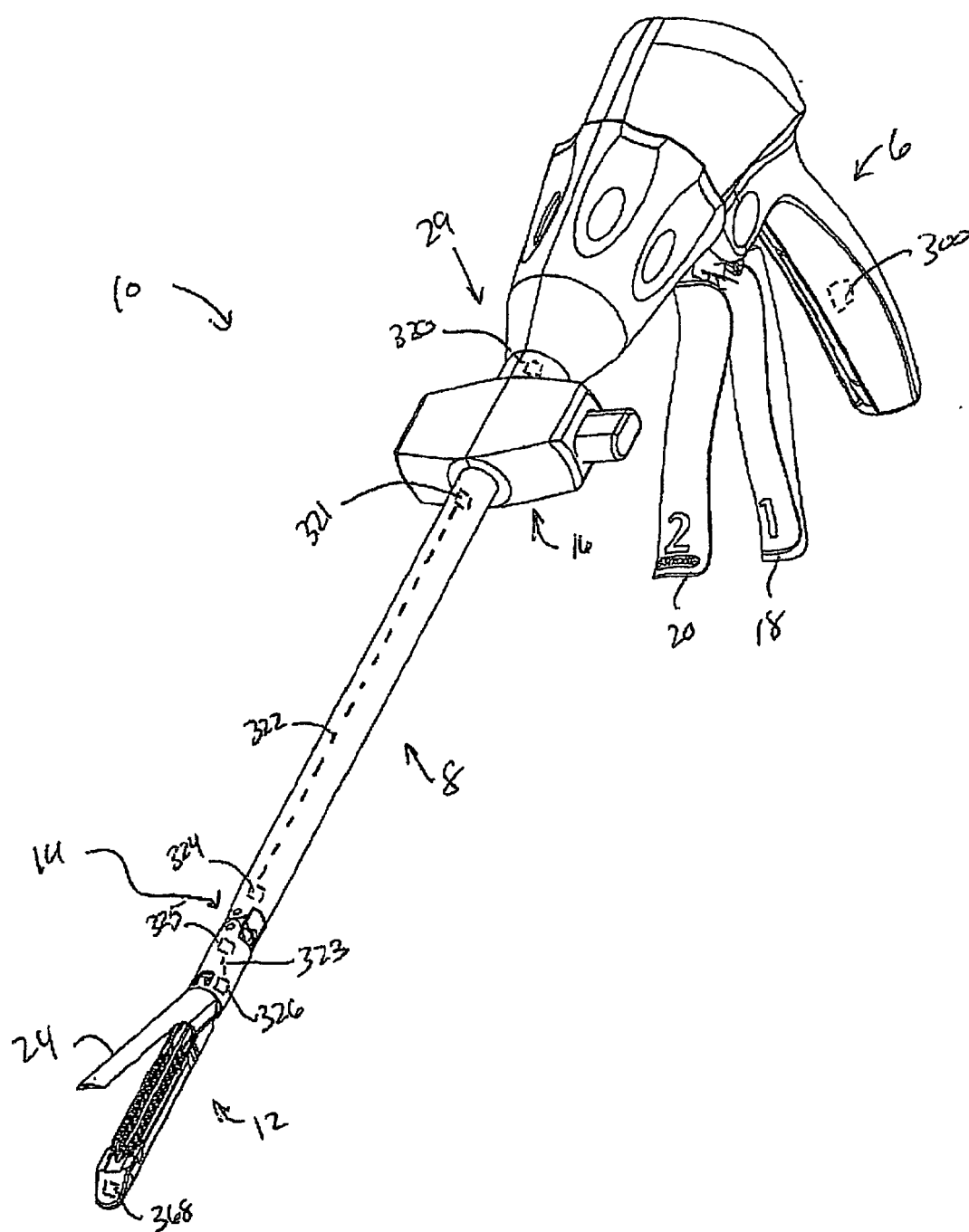
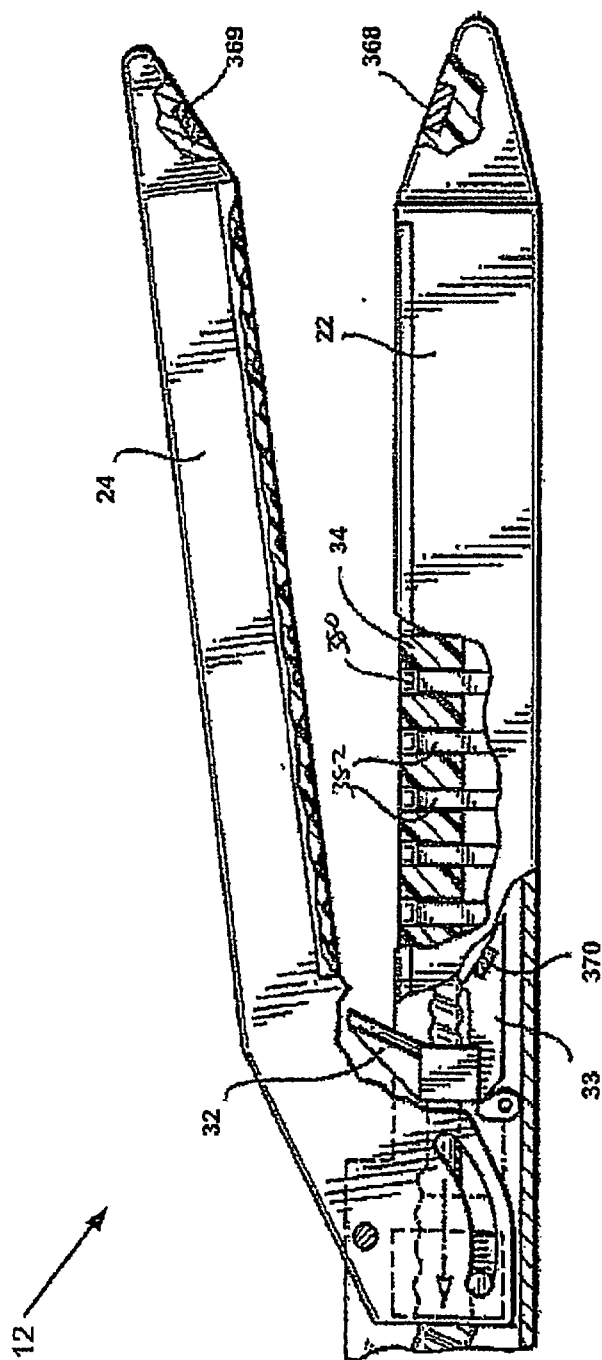


FIG. 14

FIG. 15



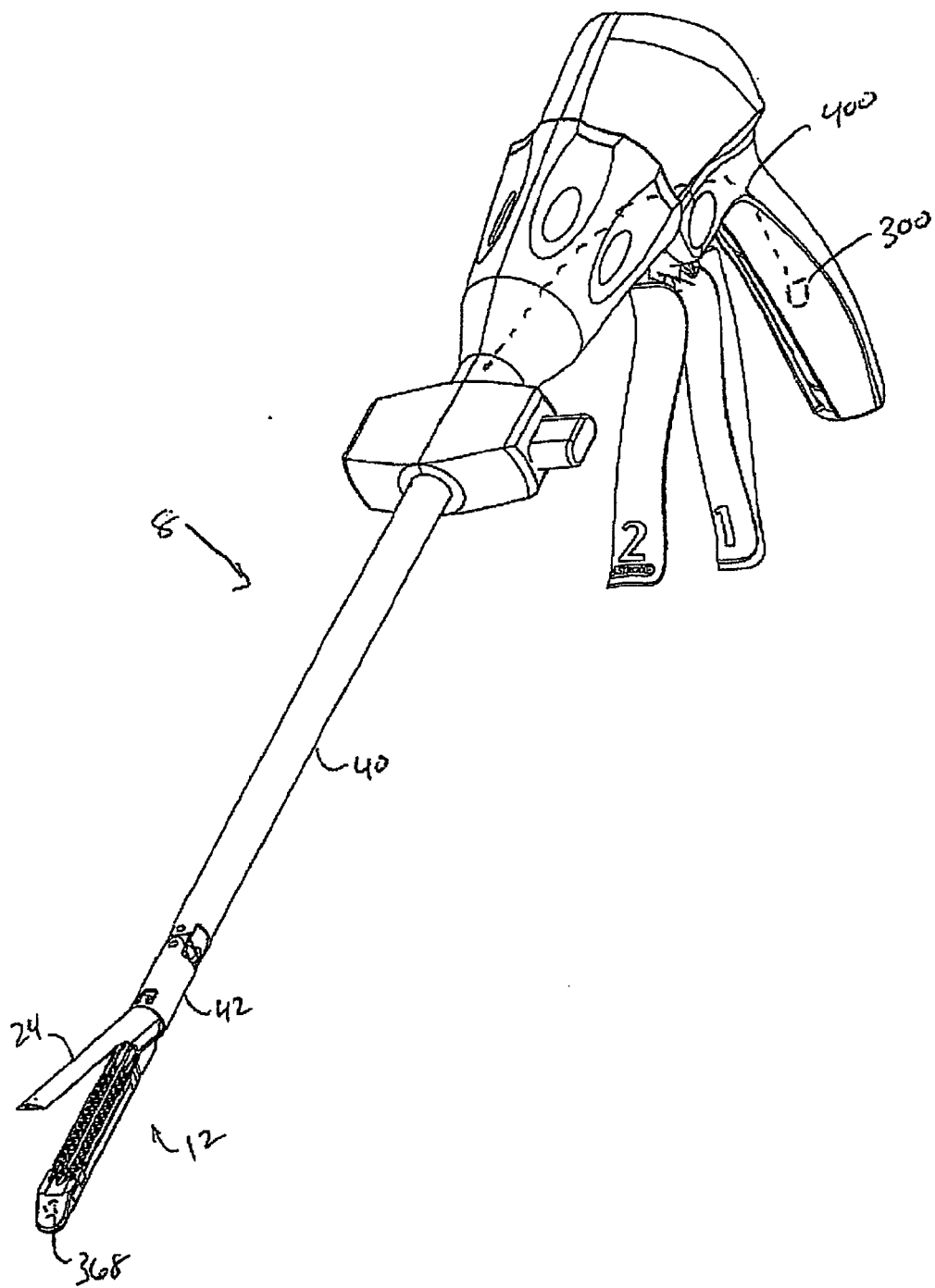


FIG. 16

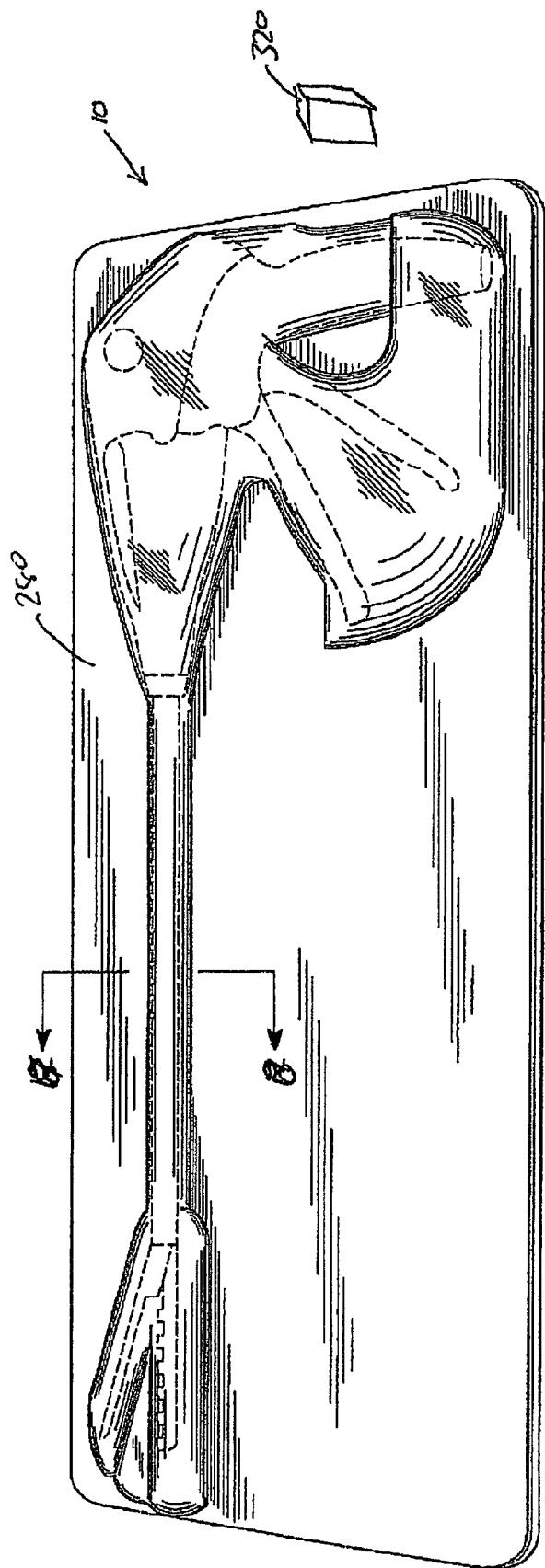


FIG. 17

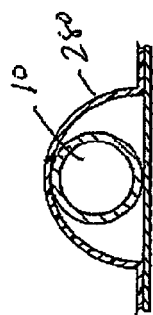


FIG. 18

Figure 19

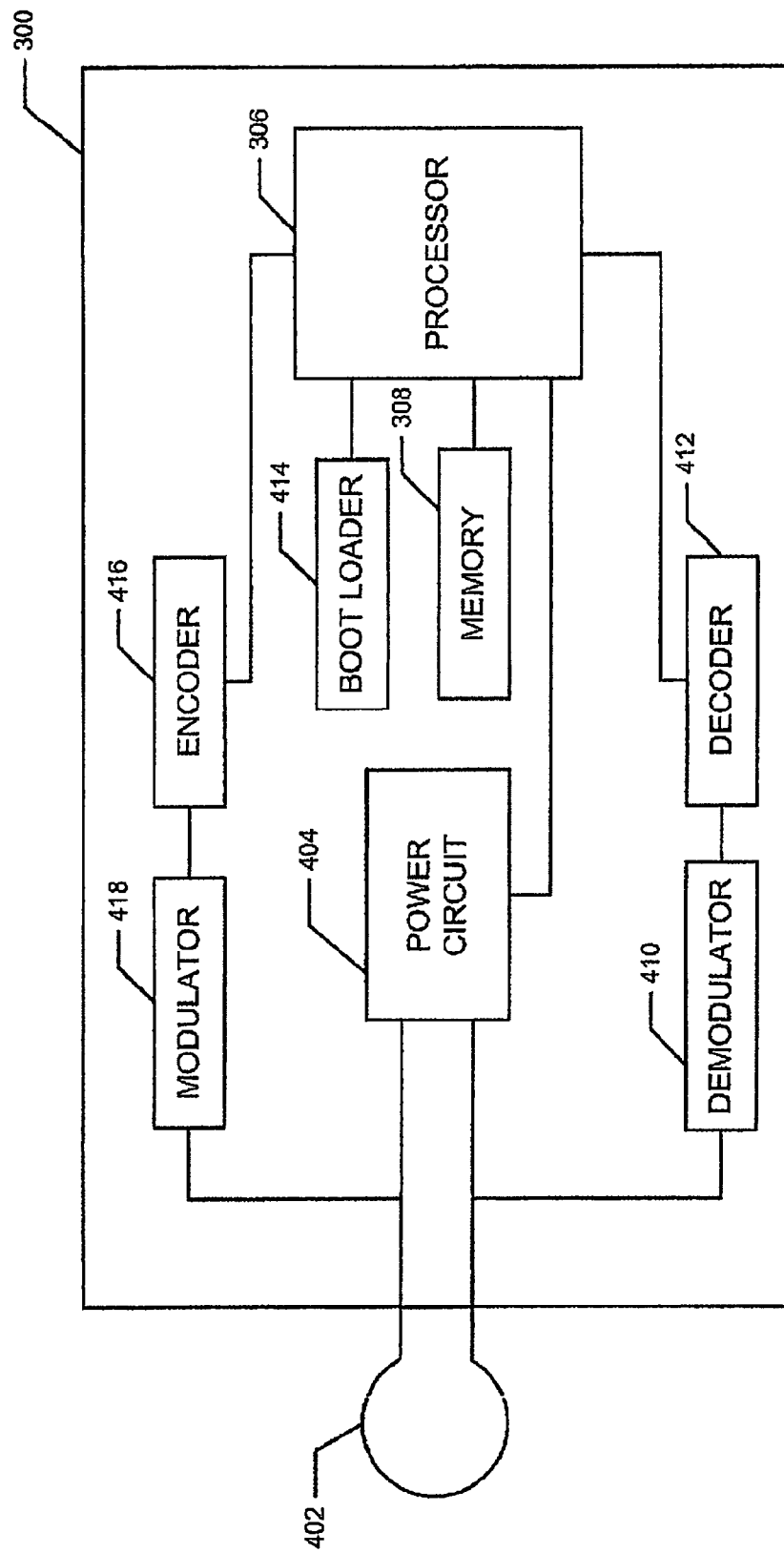
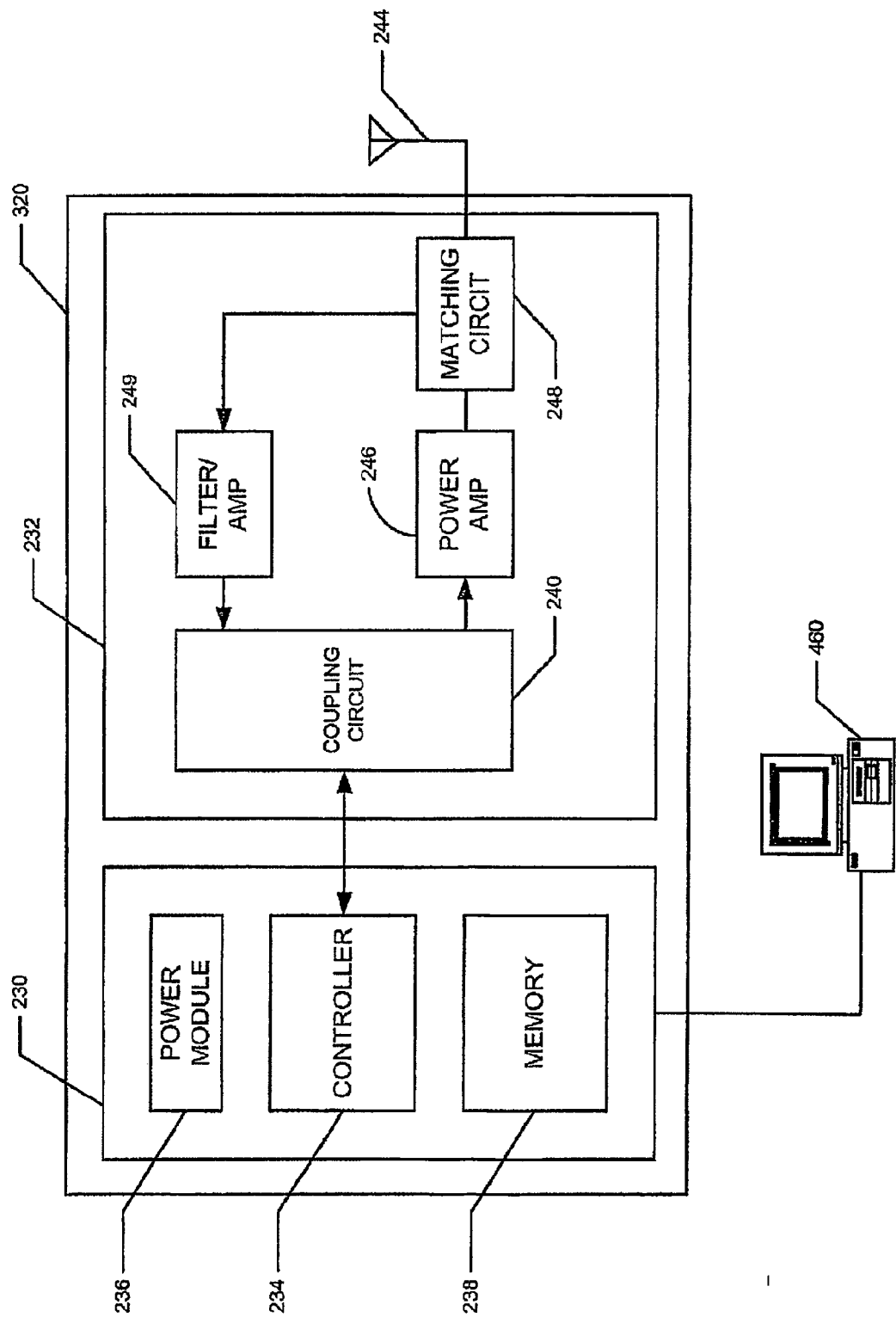


Figure 20



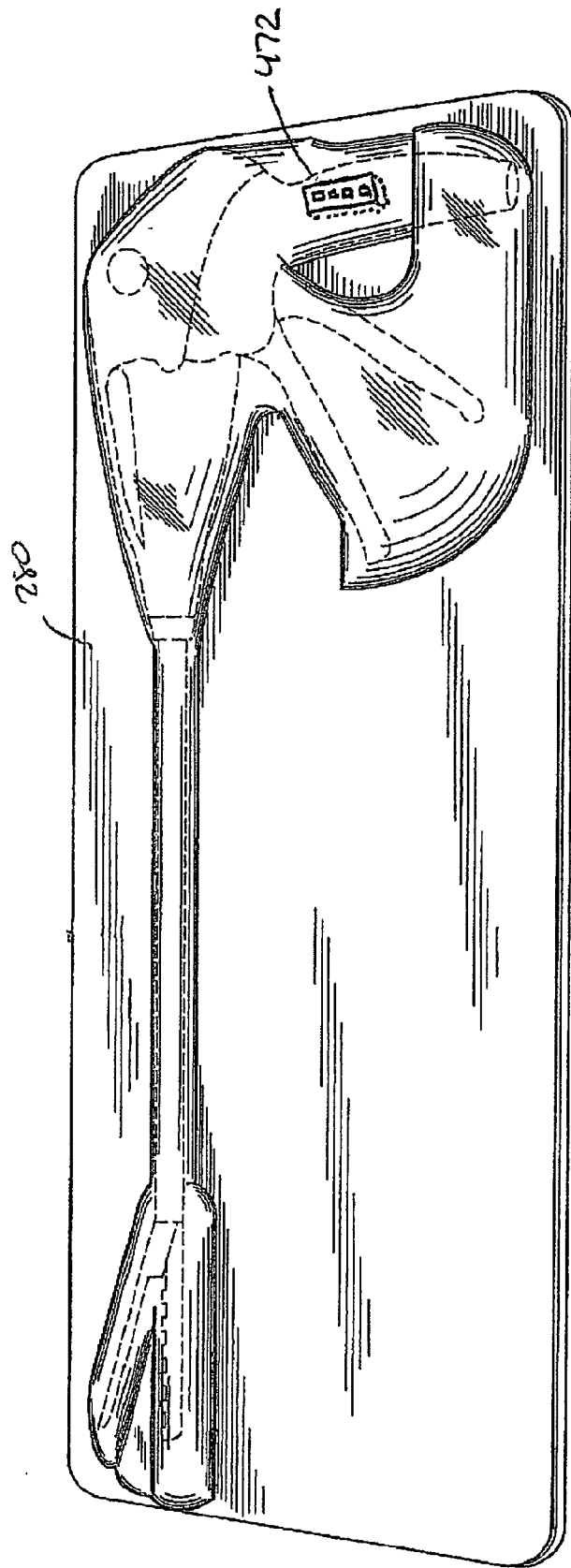


FIG. 21

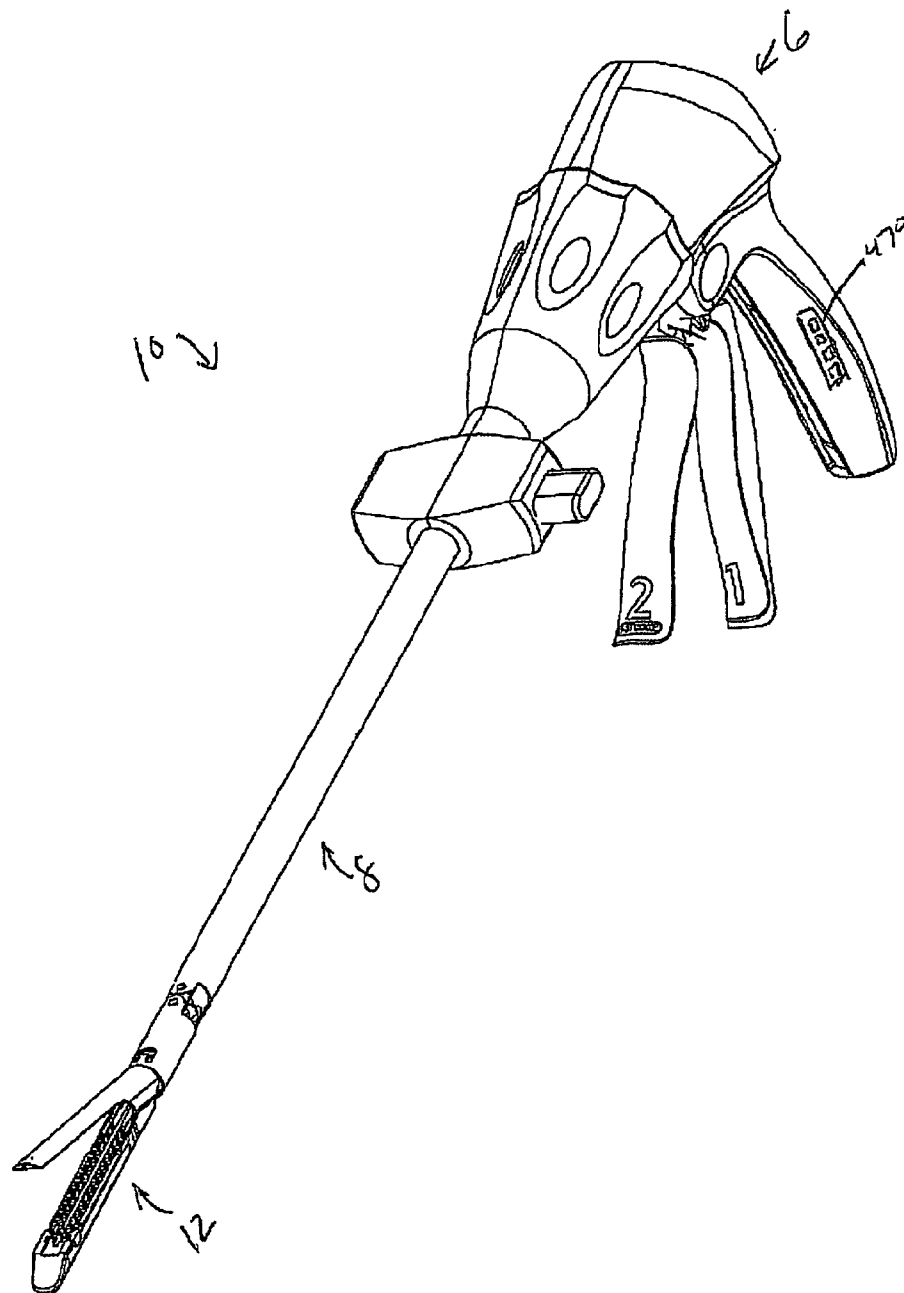


FIG. 22



EUROPEAN SEARCH REPORT

Application Number
EP 12 17 3458

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Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (IPC)
X	US 5 653 677 A (OKADA FUJIO [JP] ET AL) 5 August 1997 (1997-08-05) * column 4 - column 5; figures 1,3 *	1-7, 12-14	INV. A61B17/072
A	US 6 648 816 B2 (IRION KLAUS M [DE] ET AL) 18 November 2003 (2003-11-18) * columns 6,7 *	1,10-13	
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A	WO 03/020139 A (VLEUGELS MICHEL PETRONELLA HUB [NL]; LAZEROMS MARKUS CORNELIS JACOB [B]) 13 March 2003 (2003-03-13) * the whole document *	1-14	
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The present search report has been drawn up for all claims			
Place of search Munich		Date of completion of the search 23 November 2012	Examiner Strazdauskas, Gedas
CATEGORY OF CITED DOCUMENTS X : particularly relevant if taken alone Y : particularly relevant if combined with another document of the same category A : technological background O : non-written disclosure P : intermediate document		T : theory or principle underlying the invention E : earlier patent document, but published on, or after the filing date D : document cited in the application L : document cited for other reasons & : member of the same patent family, corresponding document	

4 EPO FORM 1503 03.82 (P04C01)

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ON EUROPEAN PATENT APPLICATION NO.**

EP 12 17 3458

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23-11-2012

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专利名称(译)	在控制单元和远程传感器之间进行无线通信的手术器械		
公开(公告)号	EP2543322A1	公开(公告)日	2013-01-09
申请号	EP2012173458	申请日	2008-01-09
[标]申请(专利权)人(译)	伊西康内外科公司		
申请(专利权)人(译)	爱惜康内镜手术，INC.		
当前申请(专利权)人(译)	ETHICON LLC		
[标]发明人	GIORDANO JAMES R SWAYZE JEFFREY S SHELTON IV FREDERICK E		
发明人	GIORDANO, JAMES R. SWAYZE, JEFFREY S. SHELTON IV, FREDERICK E.		
IPC分类号	A61B17/072		
CPC分类号	A61B17/068 A61B17/07207 A61B90/98 A61B2017/00022 A61B2017/00221 A61B2017/00398 A61B2017/00734 A61B2017/07271 A61B2017/2927 A61B2090/065 A61B2090/0814		
优先权	11/651807 2007-01-10 US		
其他公开文献	EP2543322B1		
外部链接	Espacenet		

摘要(译)

一种内窥镜或腹腔镜手术器械，包括具有至少一个传感器（368）和控制单元（300）的末端执行器（12）。手术器械还包括导电轴（40），其具有连接到末端执行器的远端。传感器与轴电绝缘，而控制单元电连接到所述轴（例如通过连杆400），使得轴配置成将来自控制单元的信号辐射到传感器并接收来自传感器的辐射信号。

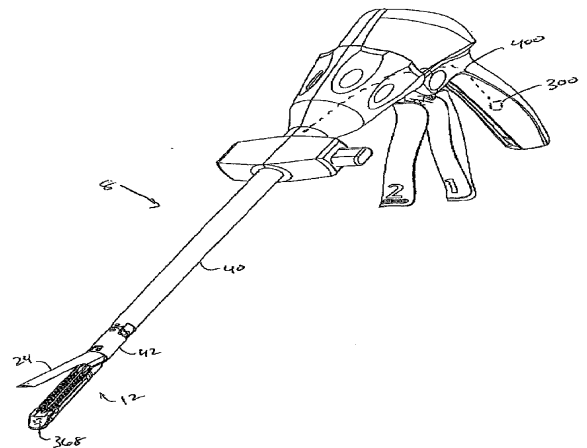


FIG. 16