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**(54) Surgical instrument with enhanced battery performance**

Chirurgisches Instrument mit verbesserter Batterieleistung

Instrument chirurgical avec une performance de batterie améliorée

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## Description

### BACKGROUND

**[0001]** Endoscopic surgical instruments are often preferred over traditional open surgical devices since a smaller incision tends to reduce the post-operative recovery time and complications. Consequently, significant development has gone into a range of endoscopic surgical instruments that are suitable for precise placement of a distal end effector at a desired surgical site through a cannula of a trocar. These distal end effectors engage the tissue in a number of ways to achieve a diagnostic or therapeutic effect (e.g., endocutter, grasper, cutter, staplers, clip applier, access device, drug/gene therapy delivery device, and energy device using ultrasound, RF, laser, etc.).

**[0002]** Known surgical staplers include an end effector that simultaneously makes a longitudinal incision in tissue and applies lines of staples on opposing sides of the incision. The end effector includes a pair of cooperating jaw members that, if the instrument is intended for endoscopic or laparoscopic applications, are capable of passing through a cannula passageway. One of the jaw members receives a staple cartridge having at least two laterally spaced rows of staples. The other jaw member defines an anvil having staple-forming pockets aligned with the rows of staples in the cartridge. The instrument includes a plurality of reciprocating wedges which, when driven distally, pass through openings in the staple cartridge and engage drivers supporting the staples to effect the firing of the staples toward the anvil.

**[0003]** An example of a surgical stapler suitable for endoscopic applications is described in U.S. Pat. No. 5,465,895, which discloses an endocutter with distinct closing and firing actions. A clinician using this device is able to close the jaw members upon tissue to position the tissue prior to firing. Once the clinician has determined that the jaw members are properly gripping tissue, the clinician can then fire the surgical stapler with a single firing stroke, thereby severing and stapling the tissue. The simultaneous severing and stapling avoids complications that may arise when performing such actions sequentially with different surgical tools that respectively only sever and staple.

**[0004]** One specific advantage of being able to close upon tissue before firing is that the clinician is able to verify via an endoscope that the desired location for the cut has been achieved, including that a sufficient amount of tissue has been captured between opposing jaws. Otherwise, opposing jaws may be drawn too close together, especially pinching at their distal ends, and thus not effectively forming closed staples in the severed tissue. At the other extreme, an excessive amount of clamped tissue may cause binding and an incomplete firing.

**[0005]** Endoscopic staplers/cutters continue to increase in complexity and function with each generation. One reason for this is the quest to lower force-to-fire

(FTF) to a level that all or a great majority of surgeons can handle. One known solution to lower FTF uses CO<sub>2</sub> or electrical motors. These devices have not fared much better than traditional hand-powered devices, but for a different reason. Surgeons typically prefer to experience proportionate force distribution to that being experienced by the end effector in the forming of the staple to assure them that the cutting/stapling cycle is complete, with the upper limit within the capabilities of most surgeons (usually around 15-30 lbs (67-133 N)). They also typically want to maintain control of deploying the staples and being able to stop at anytime if the forces felt in the handle of the device feel too great or for some other clinical reason.

**[0006]** To address this need, so-called "power-assist" endoscopic surgical instruments have been developed in which a supplemental power source aids in the firing of the instrument. For example, in some power-assist devices, a motor provides supplemental electrical power to the power input by the user from squeezing the firing trigger. Such devices are capable of providing loading force feedback and control to the operator to reduce the firing force required to be exerted by the operator in order to complete the cutting operation. One such power-assist device is described in United States Patent Application Serial No. 11/343,573, filed January 31, 2006 by Shelton et al., entitled "Motor-driven surgical cutting and fastening instrument with loading force feedback", published as U.S. Pat. No. 2007/175952.

**[0007]** Another reason for the increase in complexity and function of endoscopic surgical instruments is the quest to monitor and provide increased control over instrument components. For example, sensors and control systems are now being used to implement new functionality in surgical instruments including, for example, electronic lock-outs. For example, One such lockout device is described in United States Patent Application Serial No. 11/343,439, filed January 31, 2006 by Swayze et al., entitled, "Electronic Lockouts And Surgical Instrument Including Same", published as U.S. Pat. No. 2007/175956.

**[0008]** One challenge in using electronics in any kind of surgical instrument is providing a suitable power source. Most surgical instruments are stocked in sealed, sterilized packages. Because of this, it is usually not practical to access an instrument after it is packaged to verify the status of its power source or recharge if necessary. Accordingly, the shelf-life of the instrument is limited by the time that the power source is able to reliably hold a charge. For many kinds of instruments, though, it is desirable to choose a power source with a high peak power output. A high peak power output makes a power source more suitable for driving the motors, sensors and control systems used in surgical instruments. Sources with a high peak power output, however, such as lithium ion batteries, typically do not hold a full charge for a suitably long time. Accordingly, the choice of a power source must compromise the need for high peak power with a corre-

sponding need for a long shelf-life.

## SUMMARY

**[0009]** The present invention is directed to an assembly including a component of a surgical instrument, such as an endoscopic or laparoscopic instrument. The assembly comprises a sterile package; a surgical instrument component within the package; and a power source within the package. The power source is configured to be placed in electrical communication with the surgical instrument component. The assembly also comprise an auxiliary power source within the package and a switch, where the switch is in electrical communication with the power source and the auxiliary power source.

**[0010]** Preferred embodiments are defined in appended dependent claims 2 to 7.

**[0011]** US 6 666 875 discusses a surgical instrument that can be disinfected or sterilized, and has a rechargeable secondary battery incorporated therein. Electromagnetic energy generated by an energy generation unit located outside the surgical instrument is received by a reception coil incorporated in the surgical instrument with the surgical instrument by induction from the energy generation unit. The electromagnetic energy is then converted into charging power with which the secondary battery is recharged.

**[0012]** US 6 181 105 discusses a power source maintenance and charge system comprising: charge maintenance circuitry for maintaining a desired charge on or for charging, a special power source of a packaged device; control circuitry for actuating and de-actuating the charge maintenance circuitry; and coupling circuitry for coupling the charge maintenance circuitry to the power source including a polymer insulated flat ribbon cable that passes through one of a sterile or non-sterile sealed plastic package containing the device to connect an auxiliary power source of the charge maintenance circuitry to the special power source of the device. The two-part form of independent claim 1 is based on this document.

**[0013]** WO 2005/078892 discusses an electrically powered portable device, the device being other than a toothbrush, the device including means for providing a function to be performed by the device, an electrical power supply which incorporates at least one capacitor for storing electrical charge to power the device, electronic control circuitry to control electrical power drawn from the electrical power supply for driving the function providing means, and a recharge interface for recharging the electrical power supply, the recharge interface being arranged to be electrically connectable to a charging device.

**[0014]** US 2003/220638 discusses a device for supplying electrical energy to an electro-pen with an electric drive unit for driving a tool. The device comprises a console with an energy supply unit having an accumulator for supplying the electrical drive unit with electrical energy. The console may be configured to be sterilized by

steam having a housing and electrical components that are sealed liquid-tight. The accumulator may include a sterile covering for sterile introduction into the console. A coupling between the console and the electro-pen carries the supply of electrical energy from the console to the electro-pen. The coupling may be an electrical contact in the form of a sterilizable connector or an inductive coupling.

## FIGURES

**[0015]** Various embodiments of the present invention are described herein by way of example in conjunction with the following figures wherein:

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Figures 1 and 2 are perspective views of a surgical instrument ;

Figures 3-5 are exploded views of an end effector and shaft of a surgical instrument ;

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Figure 6 is a side view of the end effector ;

Figure 7 is an exploded view of the handle of a surgical instrument;

Figures 8 and 9 are partial perspective views of the handle;

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Figure 10 is a side view of the handle; ;

Figure 11 is a perspective view of a surgical instrument;

Figure 12 is a schematic diagram of a circuit used in a surgical instrument ;

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Figures 13 is a side view of an end effector used in a surgical instrument ;

Figures 14 and 15 show a surgical instrument in a sterile package.

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Figure 16 shows the instrument in a sterile package according to various embodiments of the present invention;

Figure 18 shows an schematic diagram of circuits used in the instrument according to an embodiment of the present invention;

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Figures 17 and 19 show two exemplary diagrams of circuits.

Figure 20 shows a component of the instrument in a sterile package according to various embodiments of the present invention; and

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Figure 21 shows a component of a surgical instrument.

## DESCRIPTION

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**[0016]** Various embodiments of the present invention are directed generally to surgical instruments and/or instrument components having power sources whose charges can be applied or maintained while the instruments and/or components are sealed in a sterile package. The present invention may be used with any type of surgical instrument comprising at least one power source, such as endoscopic or laparoscopic surgical instruments. Before describing aspects of the system, one

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type of surgical instrument in which embodiments of the present invention may be used - an endoscopic stapling and cutting instrument (*i.e.*, an endocutter) - is first described by way of illustration.

**[0017]** Figures 1 and 2 depict an endoscopic surgical instrument 10 that comprises a handle 6, a shaft 8, and an articulating end effector 12 pivotally connected to the shaft 8 at an articulation pivot 14. Correct placement and orientation of the end effector 12 may be facilitated by controls on the handle 6, including (1) a rotation knob 28 for rotating the closure tube (described in more detail below in connection with Figures 4-5) at a free rotating joint 29 of the shaft 8 to thereby rotate the end effector 12 and (2) an articulation control 16 to effect rotational articulation of the end effector 12 about the articulation pivot 14. In the illustrated instrument, the end effector 12 is configured to act as an endocutter for clamping, severing and stapling tissue, although in other configurations, different types of end effectors may be used, such as end effectors for other types of surgical instruments, such as graspers, cutters, staplers, clip appliers, access devices, drug/gene therapy devices, ultrasound, RF or laser devices, *etc.*

**[0018]** The handle 6 of the instrument 10 may include a closure trigger 18 and a firing trigger 20 for actuating the end effector 12. It will be appreciated that instruments having end effectors directed to different surgical tasks may have different numbers or types of triggers or other suitable controls for operating the end effector 12. The end effector 12 is shown separated from the handle 6 by the preferably elongate shaft 8. In one example, a clinician or operator of the instrument 10 may articulate the end effector 12 relative to the shaft 8 by utilizing the articulation control 16, as described in more detail in pending U.S. patent application Ser. No. 11/329,020, filed January 10, 2006, entitled "Surgical Instrument Having An Articulating End Effector," by Geoffrey C. Hueil *et al.*, published as U.S. Pat. No. 2007/158385.

**[0019]** In this example, the end effector 12 includes, among other things, a staple channel 22 and a pivotally translatable clamping member, such as an anvil 24, which are maintained at a spacing that assures effective stapling and severing of tissue clamped in the end effector 12. The handle 6 includes a pistol grip 26 towards which a closure trigger 18 is pivotally drawn by the clinician to cause clamping or closing of the anvil 24 toward the staple channel 22 of the end effector 12 to thereby clamp tissue positioned between the anvil 24 and channel 22. The firing trigger 20 is farther outboard of the closure trigger 18. Once the closure trigger 18 is locked in the closure position, the firing trigger 20 may rotate slightly toward the pistol grip 26 so that it can be reached by the operator using one hand. Then the operator may pivotally draw the firing trigger 20 toward the pistol grip 12 to cause the stapling and severing of clamped tissue in the end effector 12. U.S. Pat. No. 2007/175952 describes various configurations for locking and unlocking the closure trigger 18. In other configurations, different

types of clamping members besides the anvil 24 could be used, such as, for example, an opposing jaw, *etc.*

**[0020]** It will be appreciated that the terms "proximal" and "distal" are used herein with reference to a clinician gripping the handle 6 of an instrument 10. Thus, the end effector 12 is distal with respect to the more proximal handle 6. It will be further appreciated that, for convenience and clarity, spatial terms such as "vertical" and "horizontal" are used herein with respect to the drawings. However, surgical instruments are used in many orientations and positions, and these terms are not intended to be limiting and absolute.

**[0021]** The closure trigger 18 may be actuated first. Once the clinician is satisfied with the positioning of the end effector 12, the clinician may draw back the closure trigger 18 to its fully closed, locked position proximate to the pistol grip 26. The firing trigger 20 may then be actuated. The firing trigger 20 returns to the open position (shown in Figures 1 and 2) when the clinician removes pressure. A release button 30 on the handle 6, and in this example, on the pistol grip 26 of the handle, when depressed may release the locked closure trigger 18.

**[0022]** Figure 3 is an exploded view of the end effector 12. As shown in the illustrated configuration, the end effector 12 may include, in addition to the previously-mentioned channel 22 and anvil 24, a cutting instrument 32, a sled 33, a staple cartridge 34 that is removably seated in the channel 22, and a helical screw shaft 36.

The cutting instrument 32 may be, for example, a knife. The anvil 24 may be pivotally opened and closed at a pivot point 25 connected to the proximate end of the channel 22. The anvil 24 may also include a tab 27 at its proximate end that is inserted into a component of the mechanical closure system (described further below) to open and close the anvil 24. When the closure trigger 18 is actuated, that is, drawn in by a user of the instrument 10, the anvil 24 may pivot about the pivot point 25 into the clamped or closed position. If clamping of the end effector 12 is satisfactory, the operator may actuate the firing trigger 20, which, as explained in more detail below, causes the knife 32 and sled 33 to travel longitudinally along the channel 22, thereby cutting tissue clamped within the end effector 12. The movement of the sled 33 along the channel 22 causes the staples of the staple cartridge 34 to be driven through the severed tissue and against the closed anvil 24, which turns the staples to fasten the severed tissue. U.S. Pat. 6,978,921, entitled "Surgical stapling instrument incorporating an E-beam firing mechanism," provides more details about such two-stroke cutting and fastening instruments. The sled 33 may be part of the cartridge 34, such that when the knife 32 retracts following the cutting operation, the sled 33 does not retract. The channel 22 and the anvil 24 may be made of an electrically conductive material (such as metal) and in various configurations may serve as part of an antenna for communication with sensor(s) in the end effector. The cartridge 34 could be made of a non-conductive material (such as plastic) and the sensor may

be connected to or disposed in the cartridge 34, as described further below.

**[0023]** It should be noted that, although the instrument 10 described herein employ an end effector 12 that staples the severed tissue, in other examples different techniques for fastening or sealing the severed tissue may be used. For example, end effectors that use RF energy or adhesives to fasten the severed tissue may also be used. U.S. Patent No. 5,709,680, entitled "Electrosurgical Hemostatic Device" to Yates *et al.*, and U.S. Patent No. 5,688,270, entitled "Electrosurgical Hemostatic Device With Recessed And/Or Offset Electrodes" to Yates *et al.*, disclose cutting instruments that use RF energy to fasten the severed tissue. U.S. Patent Application Serial No. 11/267,811 to Morgan *et al.*, published as U.S. Pat. No. 2007/102453, disclose cutting instruments that use adhesives to fasten the severed tissue. Accordingly, although the description herein refers to cutting/stapling operations and the like, it should be recognized that this is an exemplary embodiment and is not meant to be limiting. Other tissue-fastening techniques may also be used.

**[0024]** Figures 4 and 5 are exploded views and Figure 6 is a side view of the end effector 12 and shaft 8 according to various examples. As shown in the illustrated example, the shaft 8 may include a proximate closure tube 40 and a distal closure tube 42 pivotably linked by a pivot links 44. The distal closure tube 42 includes an opening 45 into which the tab 27 on the anvil 24 is inserted in order to open and close the anvil 24. Disposed inside the closure tubes 40, 42 may be a proximate spine tube 46. Disposed inside the proximate spine tube 46 may be a main rotational (or proximate) drive shaft 48 that communicates with a secondary (or distal) drive shaft 50 via a bevel gear assembly 52. The secondary drive shaft 50 is connected to a drive gear 54 that engages a proximate drive gear 56 of the helical screw shaft 36. The vertical bevel gear 52b may sit and pivot in an opening 57 in the distal end of the proximate spine tube 46. A distal spine tube 58 may be used to enclose the secondary drive shaft 50 and the drive gears 54, 56. Collectively, the main drive shaft 48, the secondary drive shaft 50, and the articulation assembly (e.g., the bevel gear assembly 52a-c), are sometimes referred to herein as the "main drive shaft assembly."

**[0025]** A bearing 38, positioned at a distal end of the staple channel 22, receives the helical drive screw 36, allowing the helical drive screw 36 to freely rotate with respect to the channel 22. The helical screw shaft 36 may interface a threaded opening (not shown) of the knife 32 such that rotation of the shaft 36 causes the knife 32 to translate distally or proximally (depending on the direction of the rotation) through the staple channel 22. Accordingly, when the main drive shaft 48 is caused to rotate by actuation of the firing trigger 20 (as explained in more detail below), the bevel gear assembly 52a-c causes the secondary drive shaft 50 to rotate, which in turn, because of the engagement of the drive gears 54, 56, causes the

helical screw shaft 36 to rotate, which causes the knife 32 to travel longitudinally along the channel 22 to cut any tissue clamped within the end effector. The sled 33 may be made of, for example, plastic, and may have a sloped distal surface. As the sled 33 traverses the channel 22, the sloped forward surface may push up or drive the staples in the staple cartridge 34 through the clamped tissue and against the anvil 24. The anvil 24 turns the staples, thereby stapling the severed tissue. When the knife 32 is retracted, the knife 32 and sled 33 may become disengaged, thereby leaving the sled 33 at the distal end of the channel 22.

**[0026]** According to various examples, as shown Figures 7-10, the surgical instrument may include a battery 64 in the handle 6. The illustrated example provides user-feedback regarding the deployment and loading force of the cutting instrument in the end effector 12. In addition, the instrument may use power provided by the user in retracting the firing trigger 18 to power the instrument 10 (a so-called "power assist" mode). As shown in the illustrated example, the handle 6 includes exterior lower side pieces 59, 60 and exterior upper side pieces 61, 62 that fit together to form, in general, the exterior of the handle 6. The handle pieces 59-62 may be made of an electrically nonconductive material, such as plastic. A battery 64, such as a lithium ion battery, may be provided in the pistol grip portion 26 of the handle 6. The battery 64 powers a motor 65 disposed in an upper portion of the pistol grip portion 26 of the handle 6. The battery 64 may be constructed according to any suitable construction or chemistry including, for example, a Li-ion chemistry such as  $\text{LiCoO}_2$  or  $\text{LiNiO}_2$ , a Nickel Metal Hydride chemistry, *etc.* According to various configurations, the motor 65 may be a DC brushed driving motor having a maximum rotation of, approximately, 5000 RPM to 100,000 RPM. The motor 64 may drive a  $90^\circ$  bevel gear assembly 66 comprising a first bevel gear 68 and a second bevel gear 70. The bevel gear assembly 66 may drive a planetary gear assembly 72. The planetary gear assembly 72 may include a pinion gear 74 connected to a drive shaft 76. The pinion gear 74 may drive a mating ring gear 78 that drives a helical gear drum 80 via a drive shaft 82. A ring 84 may be threaded on the helical gear drum 80. Thus, when the motor 65 rotates, the ring 84 is caused to travel along the helical gear drum 80 by means of the interposed bevel gear assembly 66, planetary gear assembly 72 and ring gear 78.

**[0027]** The handle 6 may also include a run motor sensor 110 in communication with the firing trigger 20 to detect when the firing trigger 20 has been drawn in (or "closed") toward the pistol grip portion 26 of the handle 6 by the operator to thereby actuate the cutting/stapling operation by the end effector 12. The sensor 110 may be a proportional sensor such as, for example, a rheostat or variable resistor. When the firing trigger 20 is drawn in, the sensor 110 detects the movement, and sends an electrical signal indicative of the voltage (or power) to be supplied to the motor 65. When the sensor 110 is a var-

able resistor or the like, the rotation of the motor 65 may be generally proportional to the amount of movement of the firing trigger 20. That is, if the operator only draws or closes the firing trigger 20 in a little bit, the rotation of the motor 65 is relatively low. When the firing trigger 20 is fully drawn in (or in the fully closed position), the rotation of the motor 65 is at its maximum. In other words, the harder the user pulls on the firing trigger 20, the more voltage is applied to the motor 65, causing greater rates of rotation. In another configuration, for example, the control unit (described further below) may output a PWM control signal to the motor 65 based on the input from the sensor 110 in order to control the motor 65.

**[0028]** The handle 6 may include a middle handle piece 104 adjacent to the upper portion of the firing trigger 20. The handle 6 also may comprise a bias spring 112 connected between posts on the middle handle piece 104 and the firing trigger 20. The bias spring 112 may bias the firing trigger 20 to its fully open position. In that way, when the operator releases the firing trigger 20, the bias spring 112 will pull the firing trigger 20 to its open position, thereby removing actuation of the sensor 110, thereby stopping rotation of the motor 65. Moreover, by virtue of the bias spring 112, any time a user closes the firing trigger 20, the user will experience resistance to the closing operation, thereby providing the user with feedback as to the amount of rotation exerted by the motor 65. Further, the operator could stop retracting the firing trigger 20 to thereby remove force from the sensor 100, to thereby stop the motor 65. As such, the user may stop the deployment of the end effector 12, thereby providing a measure of control of the cutting/fastening operation to the operator.

**[0029]** The distal end of the helical gear drum 80 includes a distal drive shaft 120 that drives a ring gear 122, which mates with a pinion gear 124. The pinion gear 124 is connected to the main drive shaft 48 of the main drive shaft assembly. In that way, rotation of the motor 65 causes the main drive shaft assembly to rotate, which causes actuation of the end effector 12, as described above.

**[0030]** The ring 84 threaded on the helical gear drum 80 may include a post 86 that is disposed within a slot 88 of a slotted arm 90. The slotted arm 90 has an opening 92 at its opposite end 94 that receives a pivot pin 96 that is connected between the handle exterior side pieces 59, 60. The pivot pin 96 is also disposed through an opening 100 in the firing trigger 20 and an opening 102 in the middle handle piece 104.

**[0031]** In addition, the handle 6 may include a reverse motor (or end-of-stroke sensor) 130 and a stop motor (or beginning-of-stroke) sensor 142. In various configurations, the reverse motor sensor 130 may be a limit switch located at the distal end of the helical gear drum 80 such that the ring 84 threaded on the helical gear drum 80 contacts and trips the reverse motor sensor 130 when the ring 84 reaches the distal end of the helical gear drum 80. The reverse motor sensor 130, when activated, sends a signal to the control unit which sends a signal to the

motor 65 to reverse its rotation direction, thereby withdrawing the knife 32 of the end effector 12 following the cutting operation.

**[0032]** The stop motor sensor 142 may be, for example, a normally-closed limit switch. In various configurations, it may be located at the proximate end of the helical gear drum 80 so that the ring 84 trips the switch 142 when the ring 84 reaches the proximate end of the helical gear drum 80.

**[0033]** In operation, when an operator of the instrument 10 pulls back the firing trigger 20, the sensor 110 detects the deployment of the firing trigger 20 and sends a signal to the control unit which sends a signal to the motor 65 to cause forward rotation of the motor 65 at, for example, a rate proportional to how hard the operator pulls back the firing trigger 20. The forward rotation of the motor 65 in turn causes the ring gear 78 at the distal end of the planetary gear assembly 72 to rotate, thereby causing the helical gear drum 80 to rotate, causing the ring 84 threaded on the helical gear drum 80 to travel distally along the helical gear drum 80. The rotation of the helical gear drum 80 also drives the main drive shaft assembly as described above, which in turn causes deployment of the knife 32 in the end effector 12. That is, the knife 32 and sled 33 are caused to traverse the channel 22 longitudinally, thereby cutting tissue clamped in the end effector 12. Also, the stapling operation of the end effector 12 is caused to happen in instruments where a stapling-type end effector is used.

**[0034]** By the time the cutting/stapling operation of the end effector 12 is complete, the ring 84 on the helical gear drum 80 will have reached the distal end of the helical gear drum 80, thereby causing the reverse motor sensor 130 to be tripped, which sends a signal to the control unit which sends a signal to the motor 65 to cause the motor 65 to reverse its rotation. This in turn causes the knife 32 to retract, and also causes the ring 84 on the helical gear drum 80 to move back to the proximate end of the helical gear drum 80.

**[0035]** The middle handle piece 104 includes a backside shoulder 106 that engages the slotted arm 90 as best shown in Figures 8 and 9. The middle handle piece 104 also has a forward motion stop 107 that engages the firing trigger 20. The movement of the slotted arm 90 is controlled, as explained above, by rotation of the motor 65. When the slotted arm 90 rotates CCW as the ring 84 travels from the proximate end of the helical gear drum 80 to the distal end, the middle handle piece 104 will be free to rotate CCW. Thus, as the user draws in the firing trigger 20, the firing trigger 20 will engage the forward motion stop 107 of the middle handle piece 104, causing the middle handle piece 104 to rotate CCW. Due to the backside shoulder 106 engaging the slotted arm 90, however, the middle handle piece 104 will only be able to rotate CCW as far as the slotted arm 90 permits. In that way, if the motor 65 should stop rotating for some reason, the slotted arm 90 will stop rotating, and the user will not be able to further draw in the firing trigger 20 because

the middle handle piece 104 will not be free to rotate CCW due to the slotted arm 90.

**[0036]** Components of an exemplary closure system for closing (or clamping) the anvil 24 of the end effector 12 by retracting the closure trigger 18 are also shown in Figures 7-10. In the illustrated configuration, the closure system includes a yoke 250 connected to the closure trigger 18 by a pin 251 that is inserted through aligned openings in both the closure trigger 18 and the yoke 250. A pivot pin 252, about which the closure trigger 18 pivots, is inserted through another opening in the closure trigger 18 which is offset from where the pin 251 is inserted through the closure trigger 18. Thus, retraction of the closure trigger 18 causes the upper part of the closure trigger 18, to which the yoke 250 is attached via the pin 251, to rotate CCW. The distal end of the yoke 250 is connected, via a pin 254, to a first closure bracket 256. The first closure bracket 256 connects to a second closure bracket 258. Collectively, the closure brackets 256, 258 define an opening in which the proximate end of the proximate closure tube 40 (see Figure 4) is seated and held such that longitudinal movement of the closure brackets 256, 258 causes longitudinal motion by the proximate closure tube 40. The instrument 10 also includes a closure rod 260 disposed inside the proximate closure tube 40. The closure rod 260 may include a window 261 into which a post 263 on one of the handle exterior pieces, such as exterior lower side piece 59 in the illustrated configuration, is disposed to fixedly connect the closure rod 260 to the handle 6. In that way, the proximate closure tube 40 is capable of moving longitudinally relative to the closure rod 260. The closure rod 260 may also include a distal collar 267 that fits into a cavity 269 in proximate spine tube 46 and is retained therein by a cap 271 (see Figure 4).

**[0037]** In operation, when the yoke 250 rotates due to retraction of the closure trigger 18, the closure brackets 256, 258 cause the proximate closure tube 40 to move distally (*i.e.*, away from the handle end of the instrument 10), which causes the distal closure tube 42 to move distally, which causes the anvil 24 to rotate about the pivot point 25 into the clamped or closed position. When the closure trigger 18 is unlocked from the locked position, the proximate closure tube 40 is caused to slide proximally, which causes the distal closure tube 42 to slide proximally, which, by virtue of the tab 27 being inserted in the window 45 of the distal closure tube 42, causes the anvil 24 to pivot about the pivot point 25 into the open or unclamped position. In that way, by retracting and locking the closure trigger 18, an operator may clamp tissue between the anvil 24 and channel 22, and may unclamp the tissue following the cutting/stapling operation by unlocking the closure trigger 18 from the locked position.

**[0038]** The control unit (described further below) may receive the outputs from end-of stroke and beginning-of-stroke sensors 130, 142 and the run-motor sensor 110, and may control the motor 65 based on the inputs. For

example, when an operator initially pulls the firing trigger 20 after locking the closure trigger 18, the run-motor sensor 110 is actuated. If the staple cartridge 34 is present in the end effector 12, a cartridge lockout sensor (not shown) may be closed, in which case the control unit may output a control signal to the motor 65 to cause the motor 65 to rotate in the forward direction. When the end effector 12 reaches the end of its stroke, the reverse motor sensor 130 will be activated. The control unit may receive this output from the reverse motor sensor 130 and cause the motor 65 to reverse its rotational direction. When the knife 32 is fully retracted, the stop motor sensor switch 142 is activated, causing the control unit to stop the motor 65.

**[0039]** In other configurations, rather than a proportional-type sensor 110, an on-off type sensor could be used. In such examples, the rate of rotation of the motor 65 would not be proportional to the force applied by the operator. Rather, the motor 65 would generally rotate at a constant rate. But the operator would still experience force feedback because the firing trigger 20 is geared into the gear drive train.

**[0040]** The instrument 10 may include a number of sensors in the end effector 12 for sensing various conditions related to the end effector 12, such as sensors for determining the status of the staple cartridge 34 (or other type of cartridge depending on the type of surgical instrument), user input loads, the progress of the stapler during closure and firing, a compatible surgical instrument or instruments for the cartridge 34, *etc.* The sensors may be passively powered by inductive signals, or may be powered by a remote power source, such as a battery in the end effector 12, for example. The sensor(s) could include magnetoresistive, optical, electromechanical, radio frequency identification (RFID), micro-electrical-mechanical systems (MEMS), motion or pressure sensors, for example. These sensors may be in communication with a control unit 300, which may be located in the handle 6 of the instrument 10, for example, as shown in Figure 11. The sensors may be in contact with the control unit 300 according to any suitable wired or wireless method.

**[0041]** As shown in Figure 12, according to various configurations, the control unit 300 may comprise a processor 306 and one or more memory units 308. By executing instruction codes stored in the memory 308, the processor 306 may control various components of the instrument 10, such as the motor 65 or a user display (not shown), based on inputs received from the various end effector sensors and other sensor(s) (such as the run-motor sensor 110, the end-of-stroke sensor 130, and the beginning-of-stroke sensor 142, for example). The control unit 300 may be powered by the battery 64 during surgical use of instrument 10. In configurations where the control unit 300 does not have a direct, wired connection to each of the sensors and/or motors, it may comprise an inductive element 302 (*e.g.*, a coil or antenna) for transmitting and receiving wireless signals from the various sensors/motors, *etc.* Input signals received by

the inductive element 302 acting as a receiving antenna may be demodulated by a demodulator 310 and decoded by a decoder 312. Output signals may be transmitted via the encoder 316, modulator 318 and inductive element 302. Various configurations may include separate inductive elements (not shown) for receiving and transmitting.

**[0042]** According to various alternatives, the control unit 300 may be embodied as a single component, such as a microcontroller, a system-on-chip (SoC) or a system-in-package (SIP). Alternatively, the control unit 300 may be embodied as two or more discrete components. As shown in Figure 11, the control unit 300 may be housed in the handle 6 of the instrument 10 and one or more of the sensors 368 for the instrument 10 may be located in the end effector 12. In configurations where the control unit 300 and sensors 368 communicate wirelessly, the inductive element 302 of the control unit 300 may be inductively to the transponders via one or more wires (e.g., 322) and/or secondary inductive elements (e.g., coils 320 and 324). The secondary inductive elements 320, 324 may be placed to avoid running wires through articulating joints such as rotatory joint 29, pivot 14, *etc.*

**[0043]** Figure 13 is a diagram of an end effector 12 including a sensor 368 held or embedded in the cartridge 34 at the distal end of the channel 22. The sensor 368 may be connected to the cartridge 34 by a suitable bonding material, such as epoxy. In this configuration, the sensor 368 includes a magnetoresistive sensor. The anvil 24 also includes a permanent magnet 369 at its distal end and generally facing the transponder 368. The cartridge 34 also includes a permanent magnet 370 connected to the sled 33 in this exemplary configuration. This allows the sensor 368 to detect both opening/closing of the end effector 12 (due to the permanent magnet 369 moving further or closer to the transponder as the anvil 24 opens and closes) and completion of the stapling/cutting operation (due to the permanent magnet 370 moving toward the transponder 368 as the sled 33 traverses the channel 22 as part of the cutting operation). It will be appreciated that various other sensors and/or sensor types may be included in the end effector 12 and/or cartridge 34 including, for example, the radio frequency identification (RFID) sensor 371 shown.

**[0044]** Figure 13 also shows the staples 380 and the staple drivers 382 of the staple cartridge 34. As explained previously, according to various examples, when the sled 33 traverses the channel 22, the sled 33 drives the staple drivers 382 which drive the staples 380 into the severed tissue held in the end effector 12, the staples 380 being formed against the anvil 24. As noted above, such a surgical cutting and fastening instrument is but one type of surgical instrument in which the present invention may be advantageously employed.

**[0045]** In the exemplary end effector (12) described above, the battery 64 or other suitable power source powers (at least partially) the firing operation of the instrument 10. As such, the instrument may be a so-called "power-

assist" device. should be recognized, however, that the instrument 10 need not be a power-assist device and that this is merely an example of a type of device that may utilize aspects of the present invention. For example, the instrument 10 may include a user display (such as a LCD or LED display) that is powered by the battery 64 and controlled by the control unit 300. Data from the sensor transponders 368 in the end effector 12 may be displayed on such a display.

**[0046]** Typically, surgical instruments, such as the instrument 10, are cleaned and sterilized prior to use. In one sterilization technique, the instrument 10 is placed in a closed and sealed package 280, such as a plastic and/or TYVEK container or bag, as shown in Figs. 14 and 15. The package 280 and the instrument are then placed in a field of radiation that can penetrate the package, such as gamma radiation, x-rays, or high-energy electrons. The radiation kills bacteria on the instrument 10 and in the package 280. The sterilized instrument 10 can then be stored in the sterile package 280. The sealed, sterile package 280 keeps the instrument 10 sterile until it is opened in a medical facility or some other use environment. Instead of radiation, other means of sterilizing the instrument 10 may be used, such as ethylene oxide or steam. The instrument 10 may be provided to a customer in a sterilized or un-sterilized state. When the instrument 10 is provided in an un-sterilized state, the customer may sterilize the instrument 10 in-house, or send it out to an outside contractor.

**[0047]** Figure 16 shows a view, according to an embodiment of the invention, of the instrument 10 and package 280 that also includes an auxiliary power source 402. The auxiliary power source 402 is in electrical communication with the instrument 10 (e.g., the battery 64) via a connection 404 and a circuit element (not shown). The auxiliary power source 402 may provide power for charging and/or recharging an instrument power source. The auxiliary power source 402 may be any kind of battery or other suitable power source. For example, the auxiliary power source may include a rechargeable battery, such as a lithium-ion or nickel metal hydride battery, a non-rechargeable battery, such as a Zinc/Carbon, Zn/alkaline/MnO<sub>2</sub>, Li/MnO<sub>2</sub>, Zn/Ag<sub>2</sub>O, Li/FeS<sub>2</sub>, *etc.*

**[0048]** The circuit element may regulate power transferred from the auxiliary power source 402 to the instrument 10 to ensure that the battery 64 or other power source of the instrument 10 has an appropriate charge when the instrument 10 is ready for use. Physically, the circuit element may be positioned in any suitable location including, for example, as a stand alone item within the package 280, within the auxiliary power source 402, within the instrument, *etc.* The connection 404 may be any suitable kind of connection including, for example, a direct wired connection, an inductive connection, *etc.* In an inductive connection, the connection 404 may include inductive elements in close proximity to one another. A current in a first inductive element may induce a corresponding current in a second inductive element, thus



transferring electric power across the connection 404.

**[0049]** Figure 17 shows an exemplary schematic diagram of the auxiliary power source 402 connected to an instrument power source 406 (e.g., battery 64) via a circuit element 410. The auxiliary power source 402 may charge the instrument power source 406 according to any suitable method or charging profile. For example, the circuit element 410 may comprise a direct connection (e.g., inductive or wired) between the power sources 402, 406. The auxiliary source 402 may provide a charging current to charge the instrument source 406 as its charge is dissipated, for example, as the instrument 10 sits on the shelf. Also, for example, the auxiliary power source 402 may provide a charging current based on a current state of the source instrument. As shown in Figure 18, the circuit element 410 may comprise one or more switches 412 or resistors (not shown) to monitor the charge on the instrument power source 406 and provide current from the auxiliary source 402 when the charge on the source 406 reaches a predetermined threshold. Current provided by the auxiliary power source 402 may also be regulated by various other means including, for example, by microprocessor 414 and switch network 416 as shown in Figure 19. The functions of the processor 414 may be performed by the processor 306 described above, or by any other control system of the instrument 10.

**[0050]** According to various embodiments, the auxiliary power source 402 may charge the instrument source 406 relatively quickly when the instrument 10 is ready for use. For example, referring to Figure 18, the switch 412 is left in an open position while the instrument 10 and package 280 are stocked. Accordingly, the charge on the instrument power source 406 may be allowed to degrade. When the instrument 10 is ready for use, the switch 412 closed, allowing the auxiliary power source 402 to provide a charging current to the power source 406, charging the source 406 prior to use. The switch 412 is configured to close automatically when the package 280 is opened. The switch includes a tab 405, as shown in Figure 16. The tab 405 is connected to a portion of the package 280 and configured to close the switch 412 as the package 280 is opened.

**[0051]** As described above, some exemplary end effector cartridges 34 may have sensors or other electrical components that require a power source. For example, Figure 3 shows the cartridge 34 with a power source 456. The power source 456 may be any power source suitable for operating electronics present in the cartridge and/or the end effector 12. For example, the power source 456 may include a capacitor, a battery, *etc.* The power source 456 may be positioned within the cartridge 34 in any suitable location including, for example, at a distal tip, as shown in Figure 20, and as a part of the sled 33, as shown in Figure 21.

**[0052]** End effector cartridges 34 may be stored and sterilized according to the methods described above. For example, Figure 20 shows a view of a cartridge 34 enclosed in a package 450 for sterilization. As shown, the

package 450 also includes an auxiliary power source 452. The auxiliary power source may provide power to the cartridge power source 456. Like the power source 402, the power source 452 may tend to charge or recharge a power source 456 of the cartridge 34, thus increasing the shelf-life of the cartridge 34. The auxiliary power source 452 may be linked to the cartridge 34 via a connection 454 and a circuit element (not shown) similar to the circuit element described above. The auxiliary power source 452, circuit element and cartridge power source may be linked and may charge the power source 456 according to any suitable method wired or wireless (e.g., inductive) method including, for example, those discussed above with respect to Figures 17, 18 and 19.

**[0053]** According to various embodiments, a cartridge power source 456 may have a small charge capacity. Accordingly, it may be desirable to prevent unnecessary use of this charge. For example, the cartridge power source 456 may be electrically isolated from its load until the cartridge 34 is ready for use. The cartridge 34 may include a cut-off switch or other circuit element that is closed when the cartridge 34 is installed in an end effector 12. When the cut-off switch is closed, the power source 456 may be connected to its load (e.g., any sensors or other powered electronics present in the cartridge 34).

**[0054]** The cut-off switch may be implemented in any suitable way. For example, as shown in Figure 3, the cartridge 34 may include indentations 401 that are received by corresponding protrusions (not shown) in the channel 22 when the cartridge 34 is secured into the channel 22. Switch elements may be placed within these indentations 401. When the cartridge 34 is installed into the channel 22, the protrusions may be received into the indentations 401, closing the cut-off switch and connecting the power source 456 to its load. Figure 21 shows an exemplary cartridge assembly of the cut-off switch. As shown, the cut-off switch may include a pair of electrical contacts 462 positioned on a sidewall of the cartridge 34. When the cartridge 34 is secured within the channel 22 (see Figure 3), the contacts 462 are shorted by the conductive sidewall of the channel 22, closing the switch and connecting the power source 456 to its load.

**[0055]** The various embodiments of the present invention have been described above in connection with cutting-type surgical instruments. It should be noted, however, that in other embodiments, the inventive surgical instrument disclosed herein need not be a cutting-type surgical instrument, but rather could be used in any type of surgical instrument including remote sensor transponders. For example, it could be a non-cutting endoscopic instrument, a grasper, a stapler, a clip applier, an access device, a drug/gene therapy delivery device, an energy device using ultrasound, RF, laser, *etc.* In addition, the present invention may be in laparoscopic instruments, for example.

**[0056]** The devices disclosed herein can be designed to be disposed of after a single use, or they can be designed to be used multiple times. In either case, however,

the device can be reconditioned for reuse after at least one use. Reconditioning can include any combination of the steps of disassembly of the device, followed by cleaning or replacement of particular pieces, and subsequent reassembly. In particular, the device can be disassembled, and any number of the particular pieces or parts of the device can be selectively replaced or removed in any combination. Upon cleaning and/or replacement of particular parts, the device can be reassembled for subsequent use either at a reconditioning facility, or by a surgical team immediately prior to a surgical procedure. Those skilled in the art will appreciate that reconditioning of a device can utilize a variety of techniques for disassembly, cleaning/replacement, and reassembly. Use of such techniques, and the resulting reconditioned device, are all within the scope of the present application.

**[0057]** Although the present invention has been described herein in connection with certain disclosed embodiments, many modifications and variations to those embodiments may be implemented. For example, different types of end effectors may be employed. Also, where materials are disclosed for certain components, other materials may be used. The following claims are intended to cover all such modification and variations.

## Claims

### 1. An assembly comprising:

a sterile package (280);  
 a surgical instrument component within the package;  
 a power source (406) within the package, wherein the power source is configured to be placed in electrical communication with the surgical instrument component;  
 an auxiliary power source (402) within the package; and  
 a switch (412) in electrical communication with the power source and the auxiliary power source,  
**characterized in that** the switch (412) comprises a tab (405) that is connected to a portion of the package (280), wherein the tab is configured to close the switch automatically when the package is opened.

2. The assembly of claim 1, wherein the power source (406) is a battery (64).

3. The assembly of claim 1, wherein the battery (64) comprises at least one cell selected from the group consisting of a lithium ion cell and a nickel metal hydride cell.

4. The assembly of claim 1, wherein the power source (406) is a capacitor.

5. The assembly of claim 1, wherein the surgical instrument component comprises an endocutter (10).

6. The assembly of claim 1, wherein the surgical instrument component comprises an end effector cartridge (34) for a surgical instrument (10).

7. The assembly of claim 1, wherein the auxiliary power source (402) comprises one of a Zinc/carbon battery, a Zn/alkaline/MnO<sub>2</sub> battery, a Li/MnO<sub>2</sub> battery, a Zn/Ag<sub>2</sub>O battery or a LiFeS<sub>2</sub> battery

## Patentansprüche

### 1. Anordnung, die Folgendes umfasst:

eine sterile Baueinheit (280);  
 eine Komponente eines chirurgischen Instruments in der Baueinheit;  
 eine Energiequelle (406) in der Baueinheit, wobei die Energiequelle konfiguriert ist, in elektrische Kommunikation mit der Komponente eines chirurgischen Instruments gebracht zu werden;  
 eine Hilfsenergiequelle (402) in der Baueinheit; und  
 einen Schalter (412) in elektrischer Kommunikation mit der Energiequelle und der Hilfsenergiequelle,  
**dadurch gekennzeichnet, dass** der Schalter (412) eine Lasche (405) umfasst, die mit einem Teil der Baueinheit (280) verbunden ist, wobei die Lasche konfiguriert ist, den Schalter automatisch zu schließen, wenn die Baueinheit geöffnet wird.

2. Anordnung nach Anspruch 1, wobei die Energiequelle (406) eine Batterie (64) ist.

3. Anordnung nach Anspruch 1, wobei die Batterie (64) mindestens eine Zelle umfasst, die aus der Gruppe gewählt wird, die besteht aus einer Lithium-Ionen-Zelle und einer Nickel-Metallhydrid-Zelle.

4. Anordnung nach Anspruch 1, wobei die Energiequelle (406) ein Kondensator ist.

5. Anordnung nach Anspruch 1, wobei die Komponente eines chirurgischen Instruments ein Endoschneidwerkzeug (10) umfasst.

6. Anordnung nach Anspruch 1, wobei die Komponente eines chirurgischen Instruments eine Endeffektorhülse (34) für ein chirurgisches Instrument (10) umfasst.

7. Anordnung nach Anspruch 1, wobei die Hilfsenergiequelle (402) eine Zink-Kohle-Batterie, eine Zink-

Alkali-Mangandioxid-Batterien, eine Lithium-Mangandioxid-Batterie, eine Silberoxid-Zink-Batterie oder eine Lithium-Eisensulfid-Batterie umfasst.

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## Revendications

### 1. Ensemble, comprenant :

un emballage stérile (280) ; 10  
 un composant d'instrument chirurgical à l'intérieur de l'emballage ;  
 une source d'alimentation (406) à l'intérieur de l'emballage, la source d'alimentation étant configurée pour être mise en liaison électrique avec le composant d'instrument chirurgical ; 15  
 une source d'alimentation auxiliaire (402) à l'intérieur de l'emballage ; et  
 un commutateur (412) en liaison électrique avec la source d'alimentation et la source d'alimentation auxiliaire, 20  
**caractérisé en ce que** le commutateur (412) comprend une languette (405) rattachée à une partie de l'emballage (280), la languette étant configurée pour fermer automatiquement le commutateur lors de l'ouverture de l'emballage. 25

### 2. Ensemble selon la revendication 1, dans lequel la source d'alimentation (406) est une pile (64).

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### 3. Ensemble selon la revendication 1, dans lequel la pile (64) comprend au moins un accumulateur choisi dans le groupe constitué par un accumulateur lithium et un accumulateur nickel-hydrure métallique.

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### 4. Ensemble selon la revendication 1, dans lequel la source d'alimentation (406) est un condensateur.

### 5. Ensemble selon la revendication 1, dans lequel le composant d'instrument chirurgical comprend une agrafeuse coupante endoscopique (10).

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### 6. Ensemble selon la revendication 1, dans lequel le composant d'instrument chirurgical comprend une cartouche (34) d'effecteur terminal pour un instrument chirurgical (10).

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### 7. Ensemble selon la revendication 1, dans lequel la source d'alimentation auxiliaire (402) comprend une pile parmi une pile zinc/carbone, une pile Zn/alcaline/MnO<sub>2</sub>, une pile Li/MnO<sub>2</sub>, une pile Zn/Ag<sub>2</sub>O ou une pile LiFeS<sub>2</sub>.

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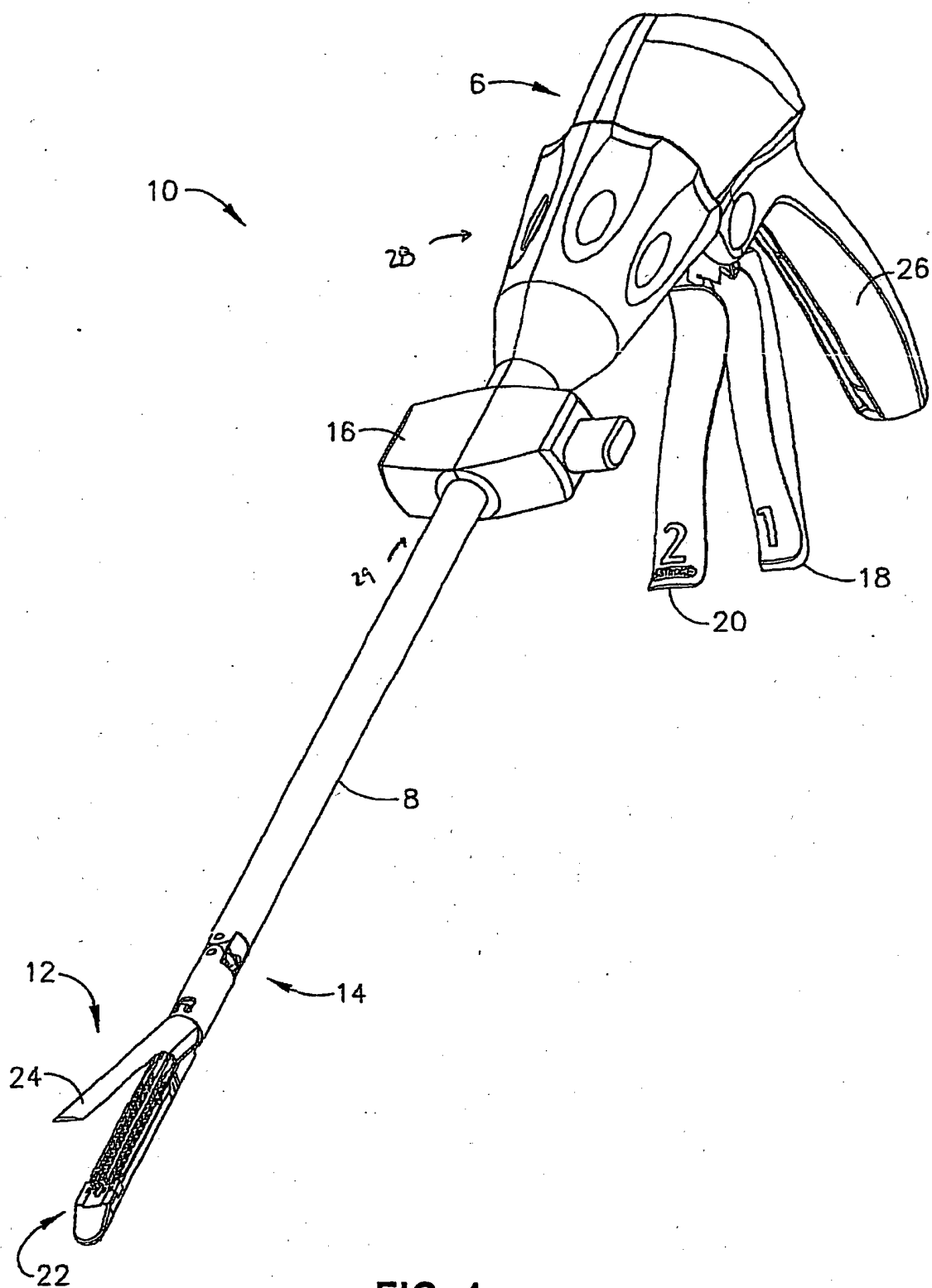


FIG. 1

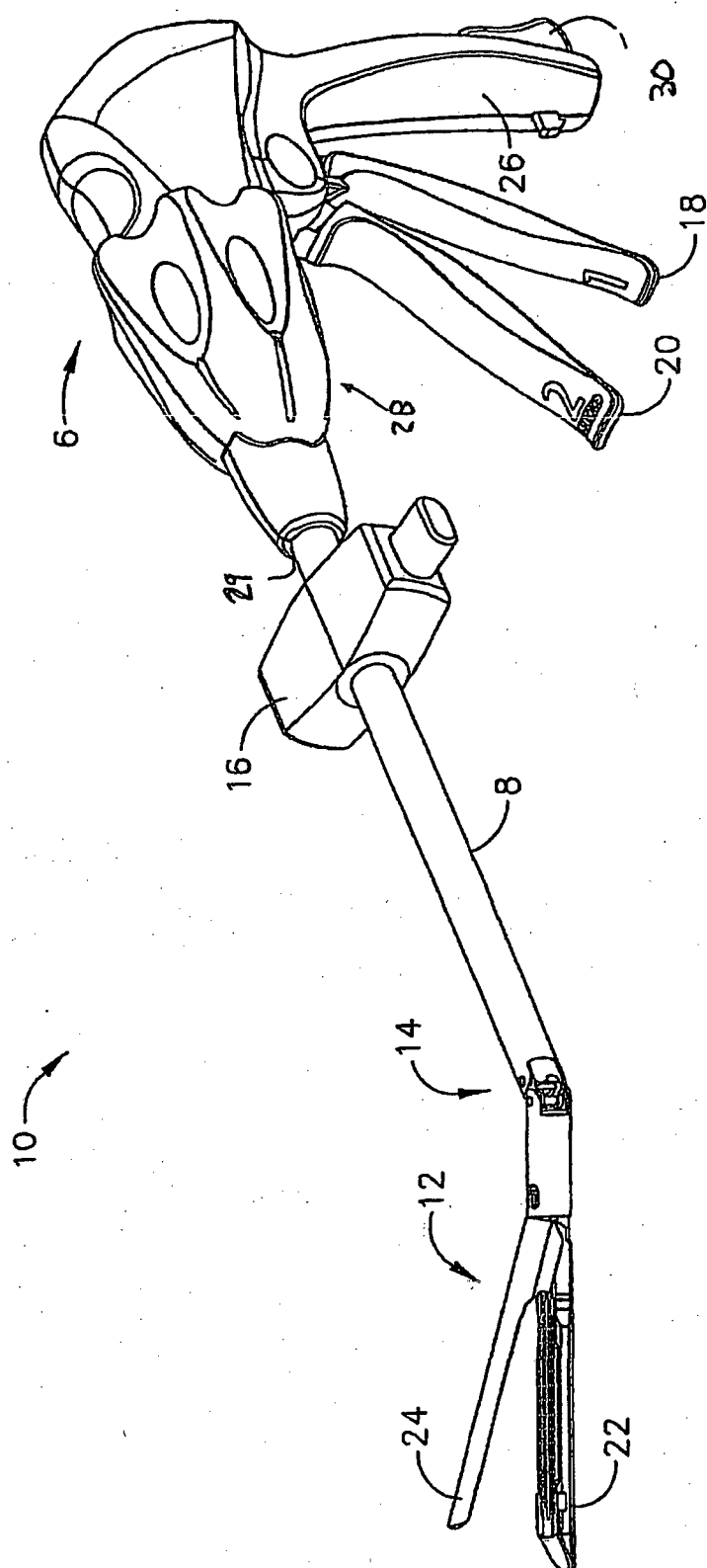


FIG. 2

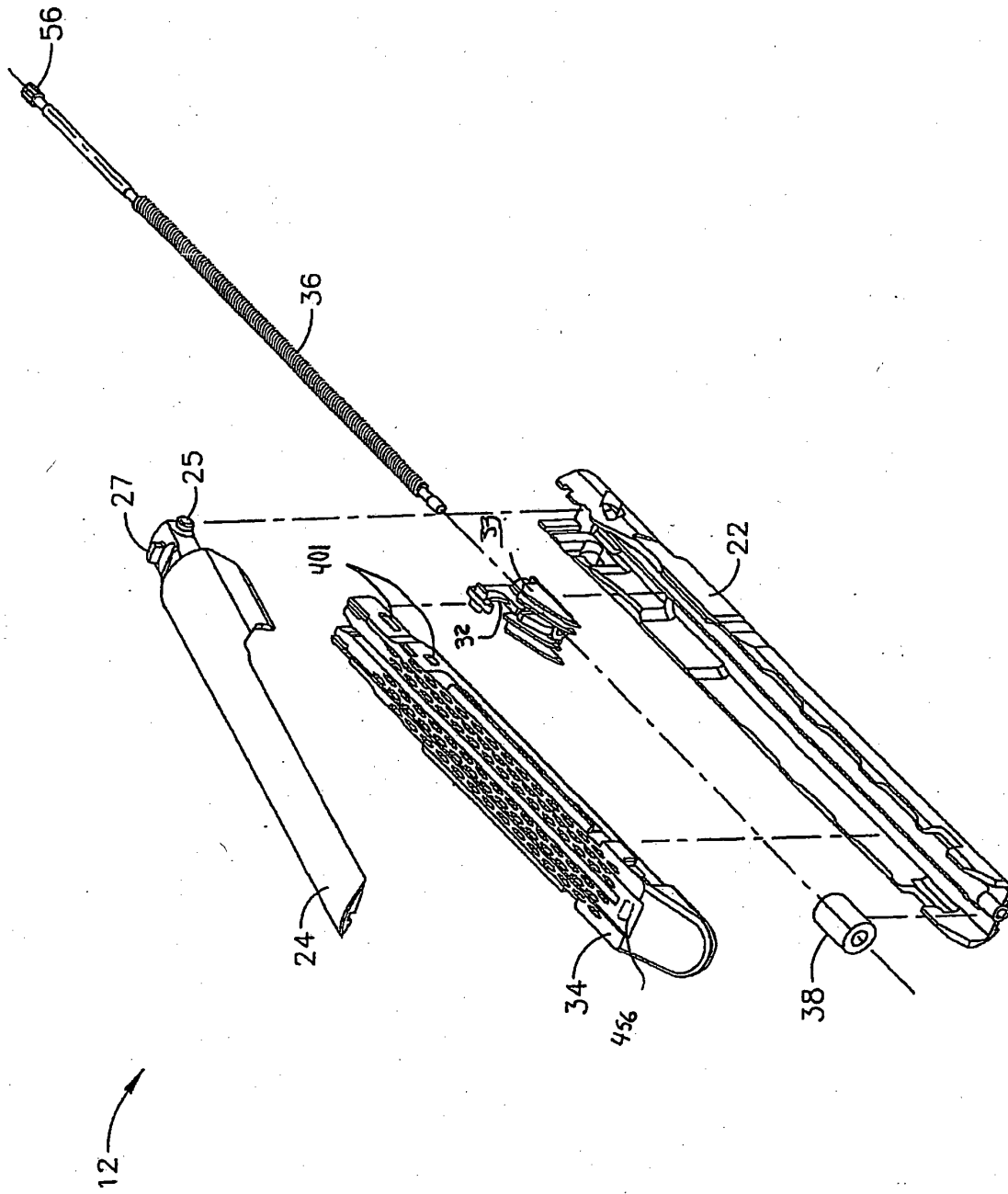


FIG. 3

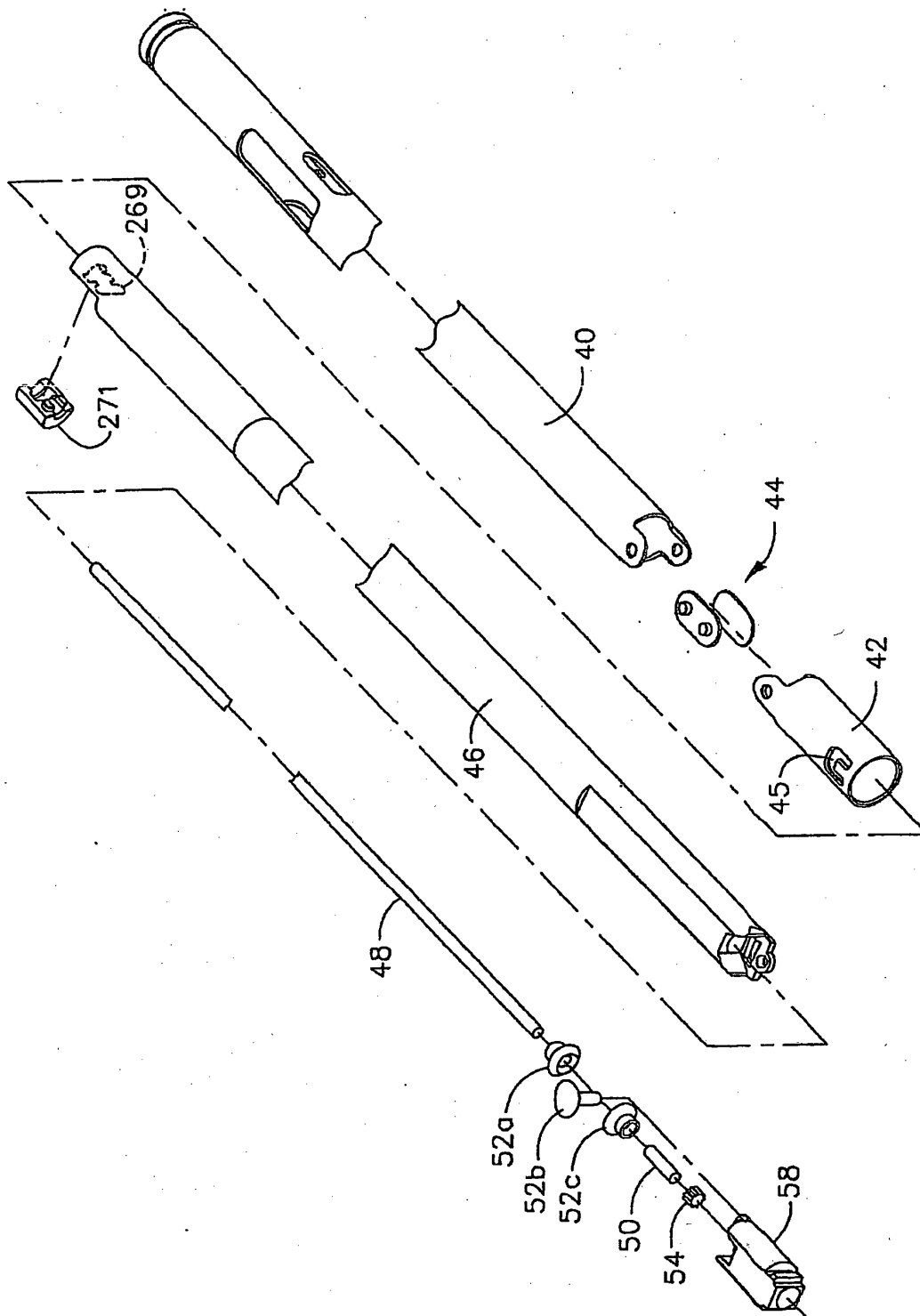


FIG. 4

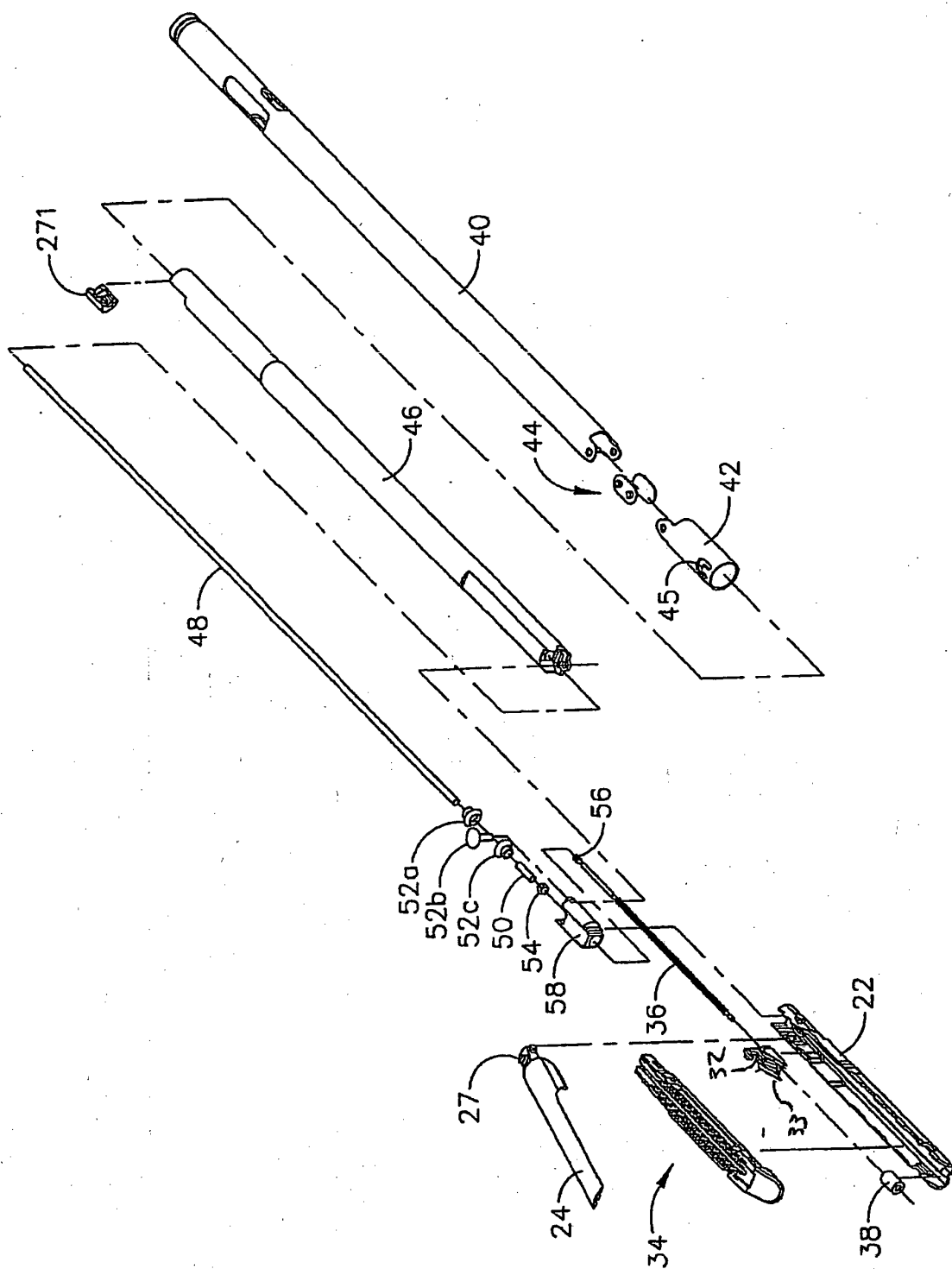


FIG. 5



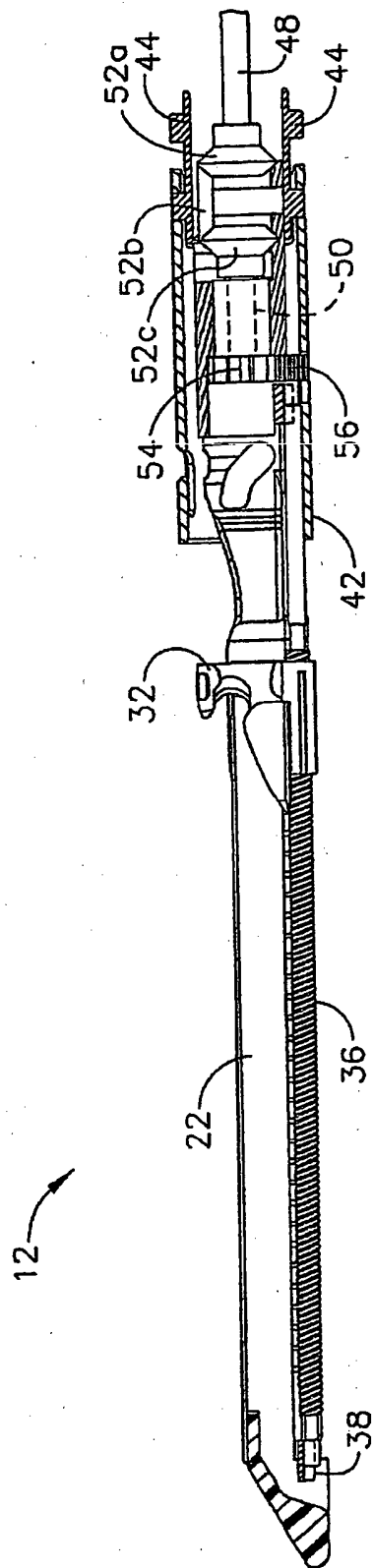


FIG. 6

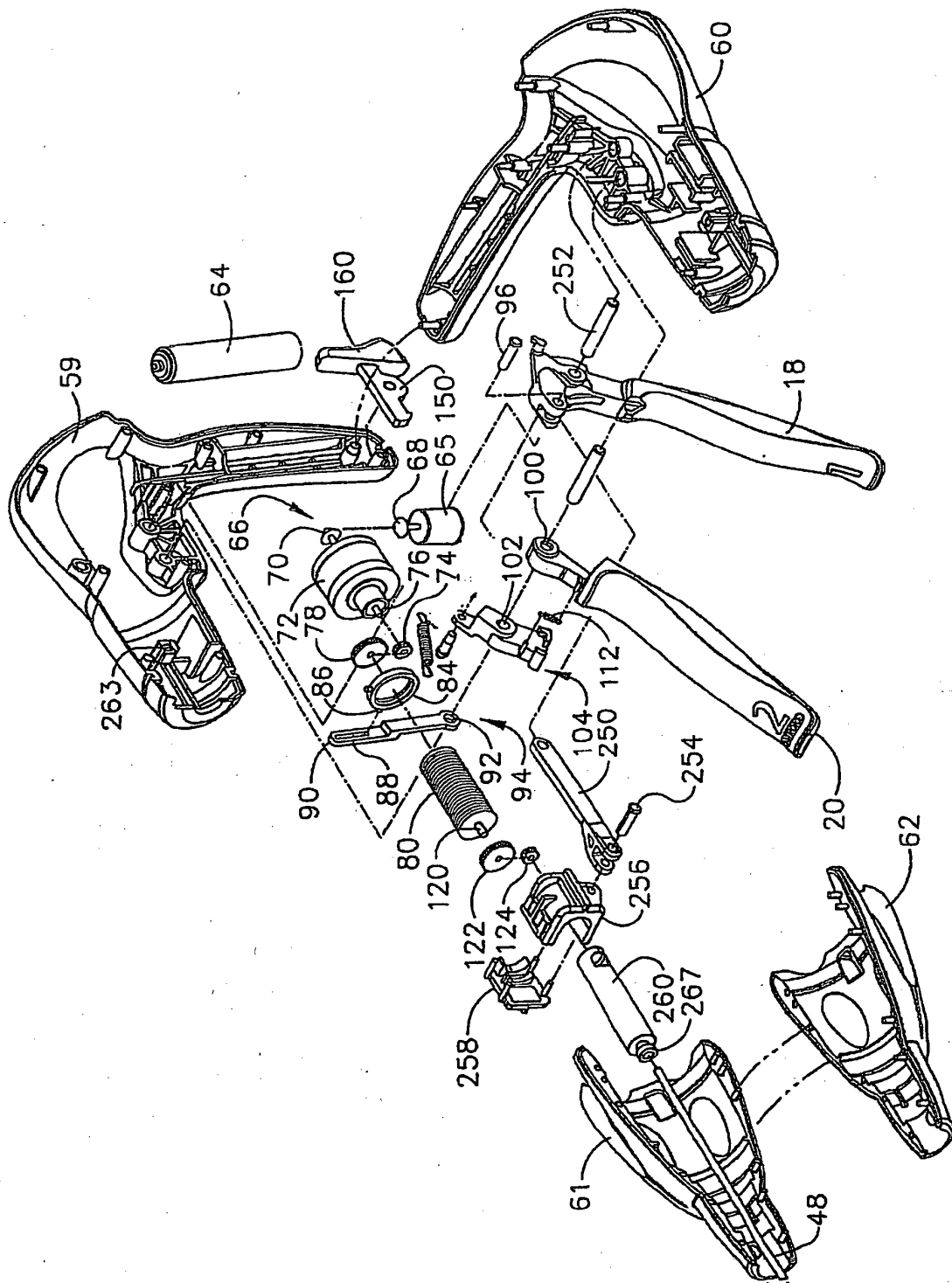


FIG. 7

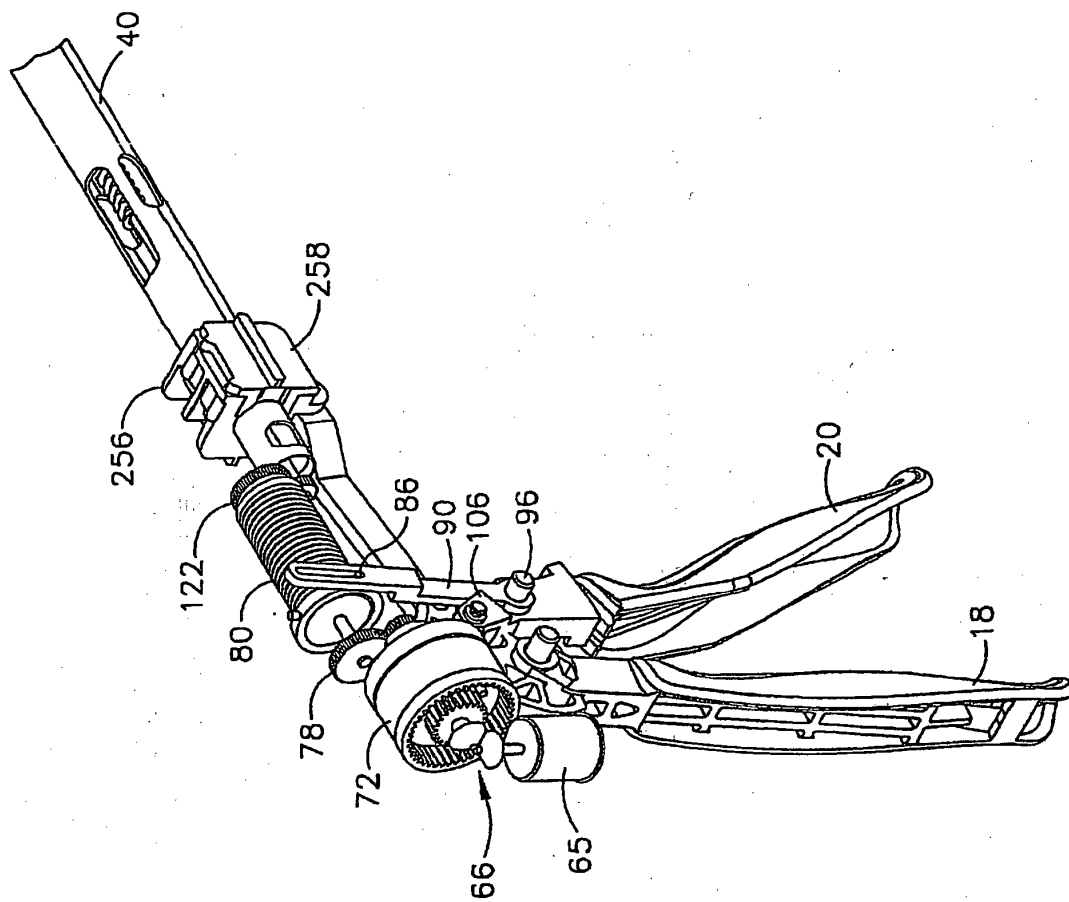


FIG. 8

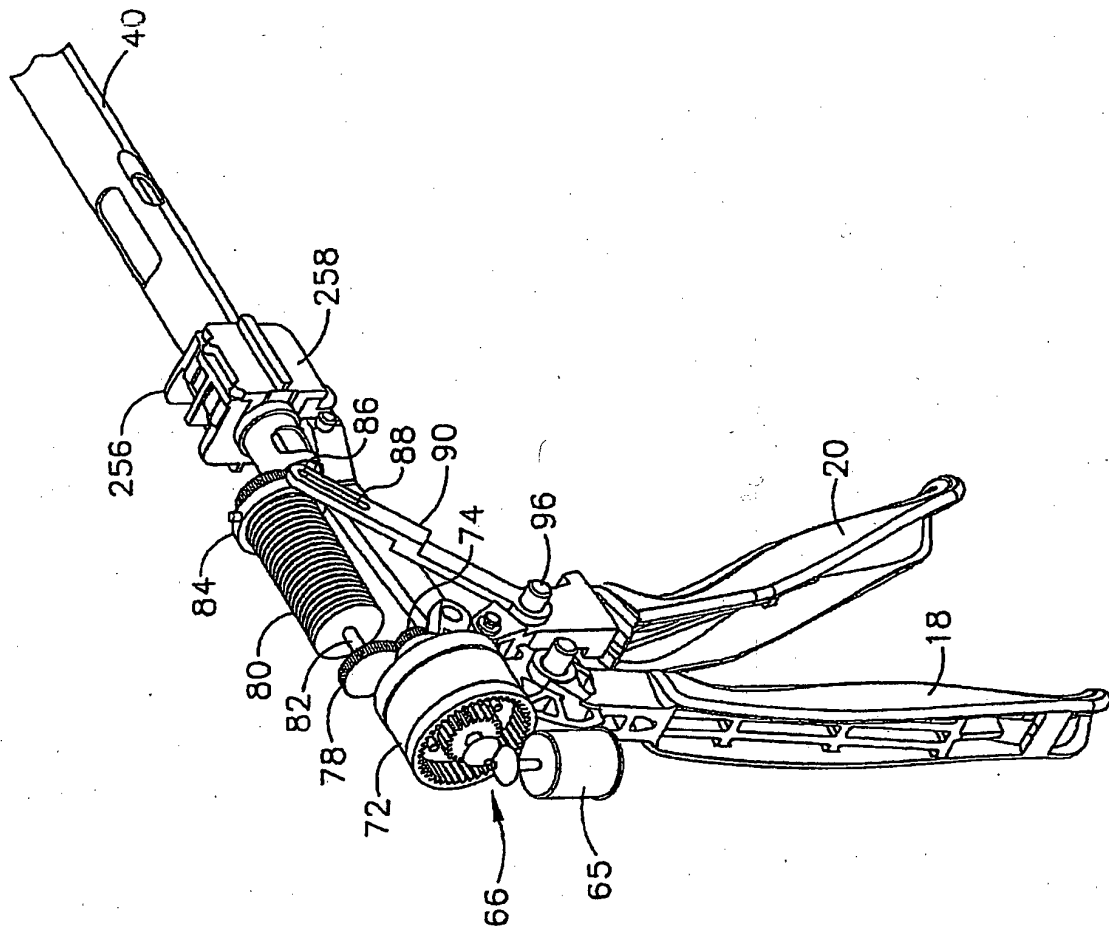


FIG. 9

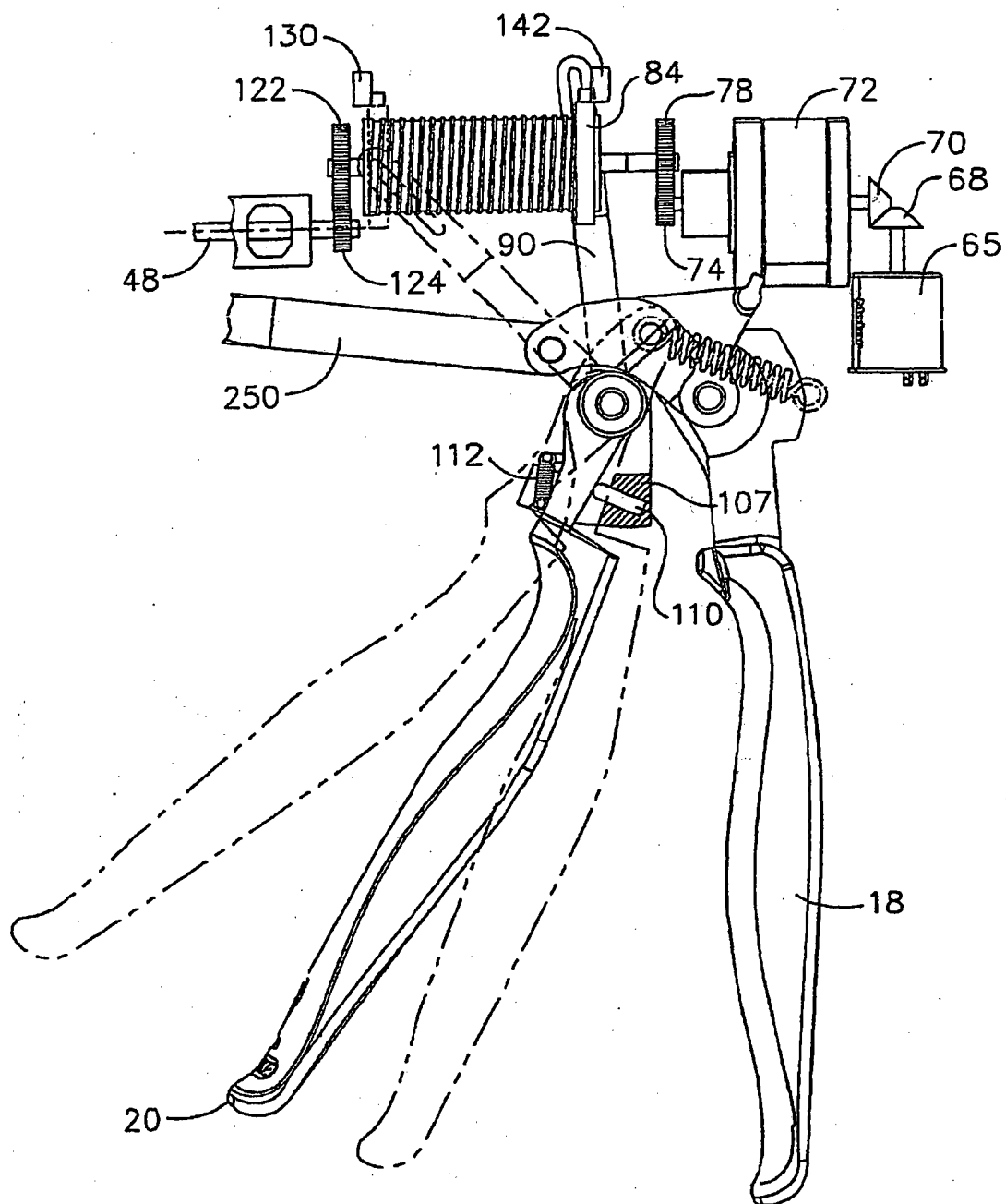


FIG. 10

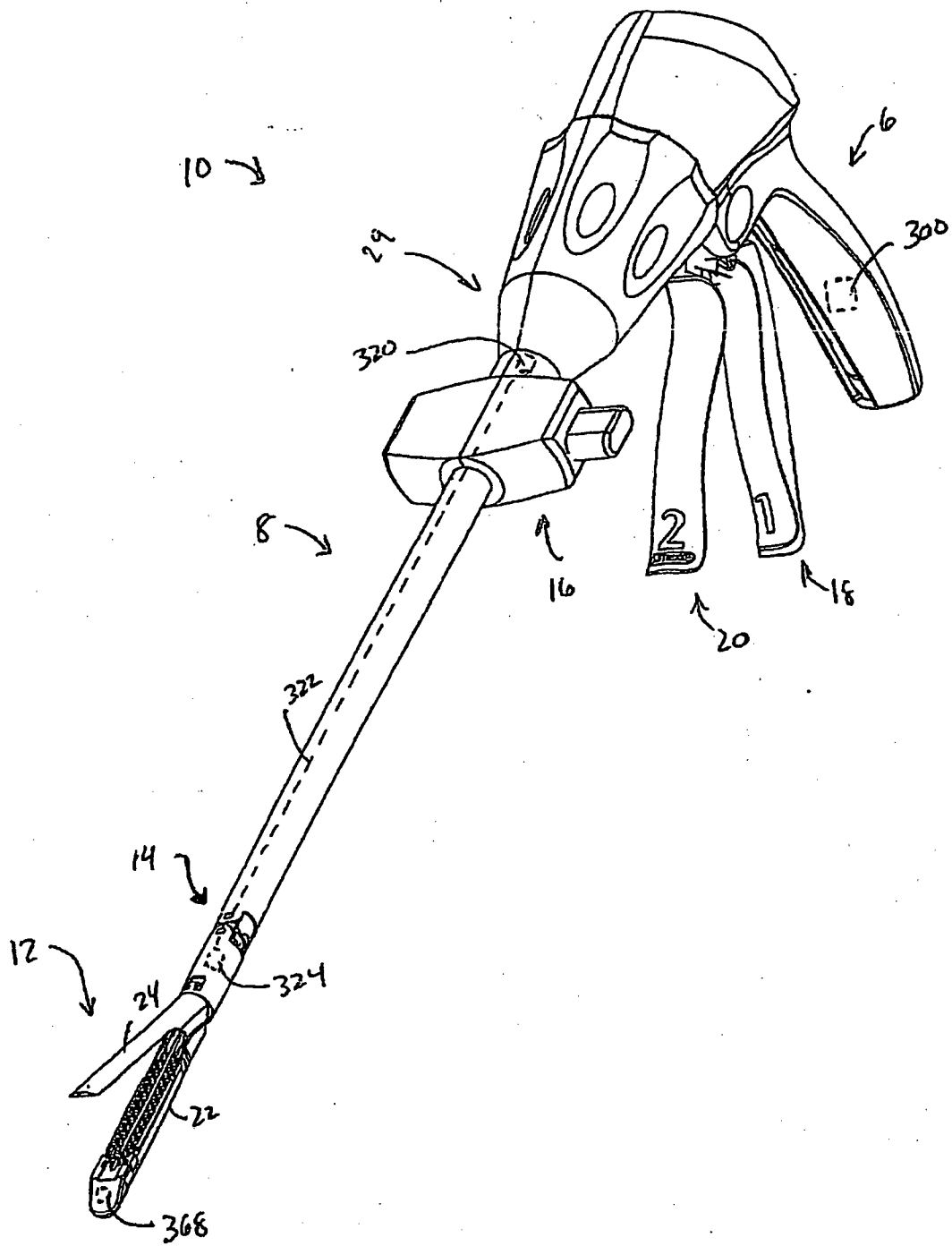


FIG. 11

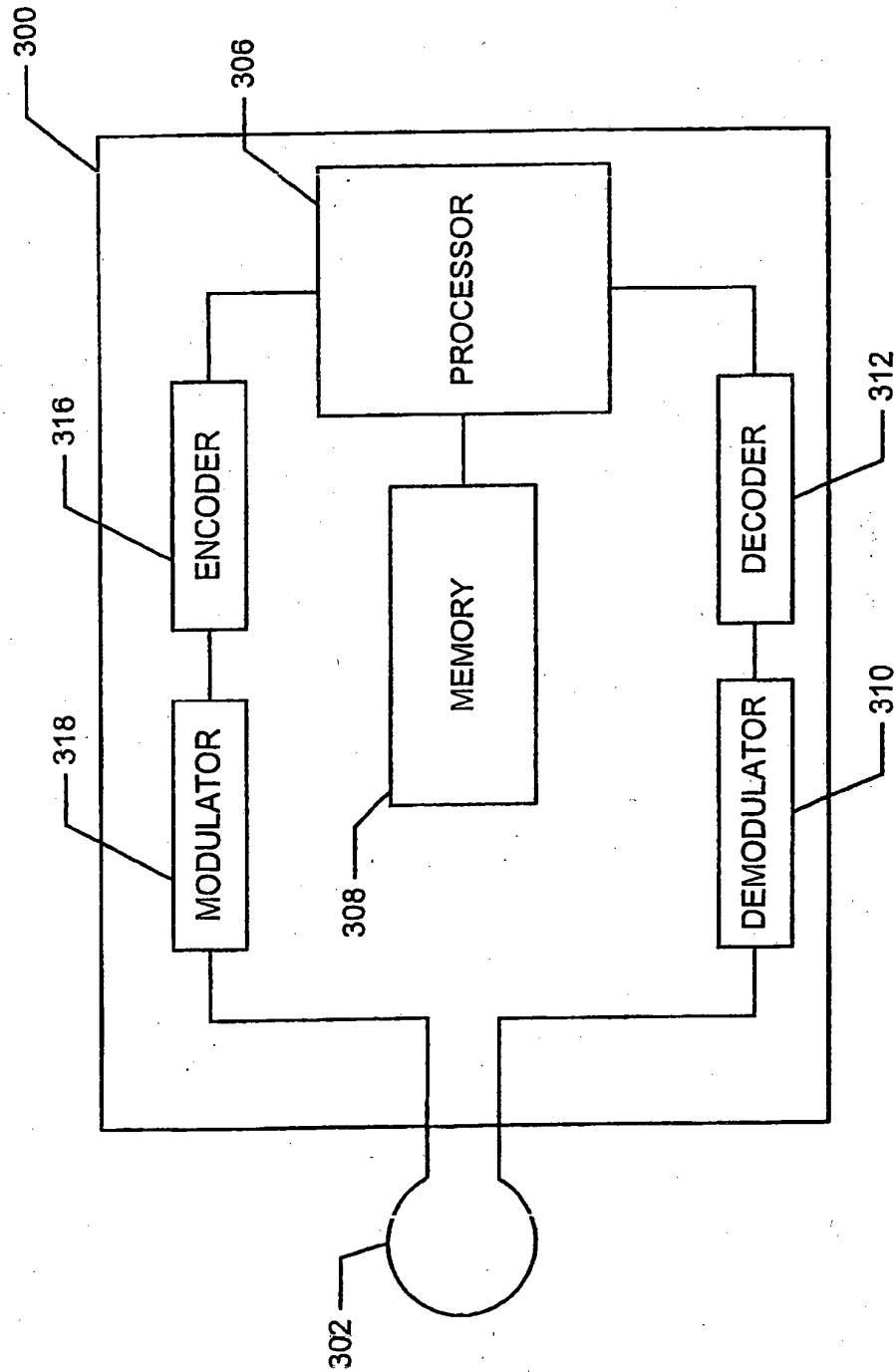


FIG. 12

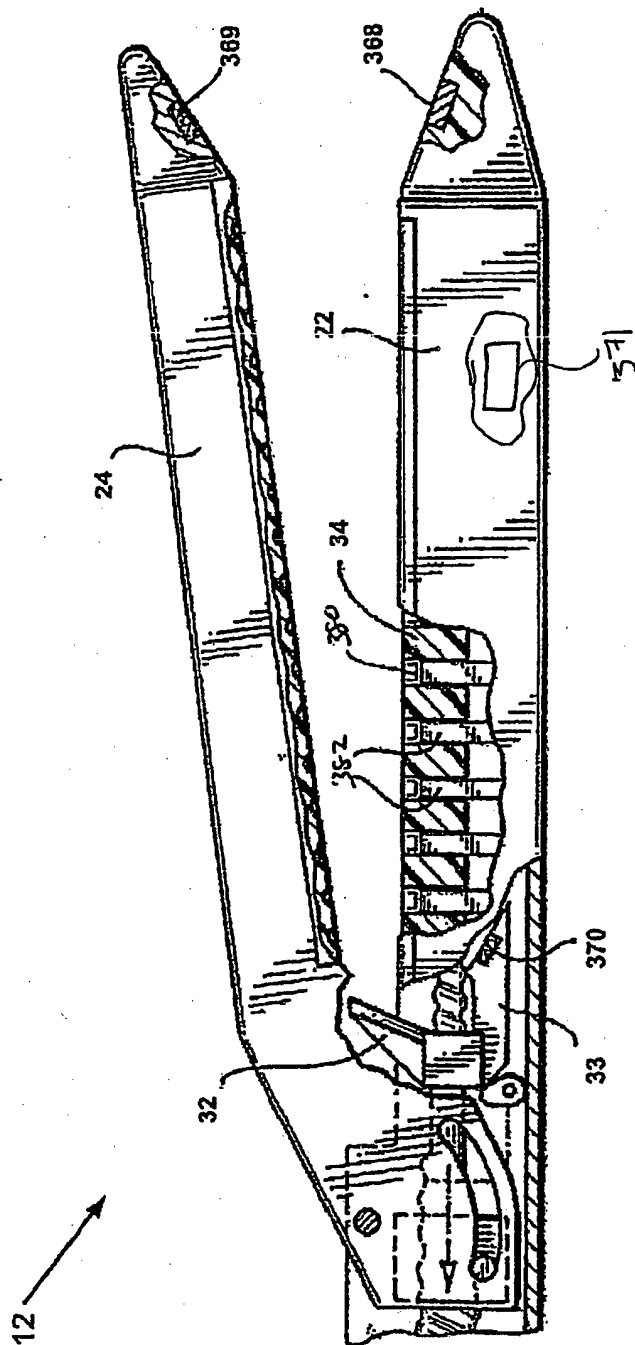


FIG. 13



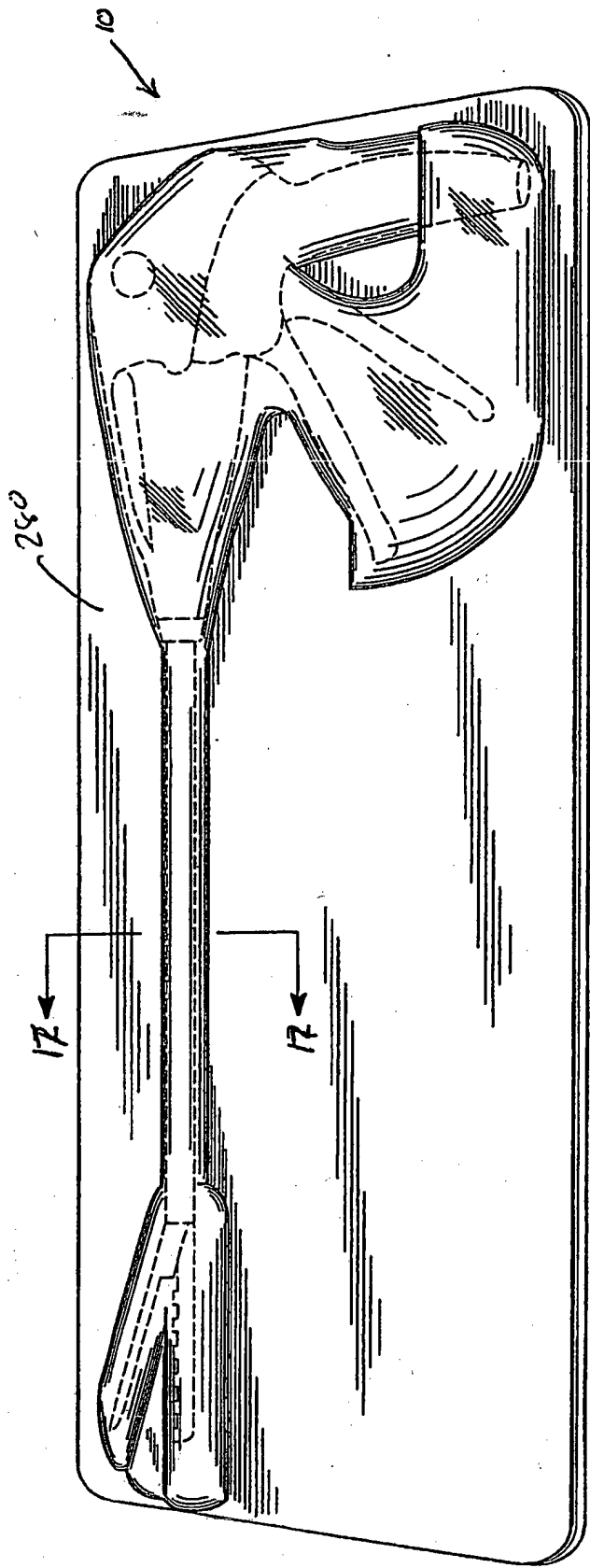


FIG. 14

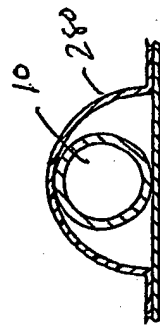


FIG. 15

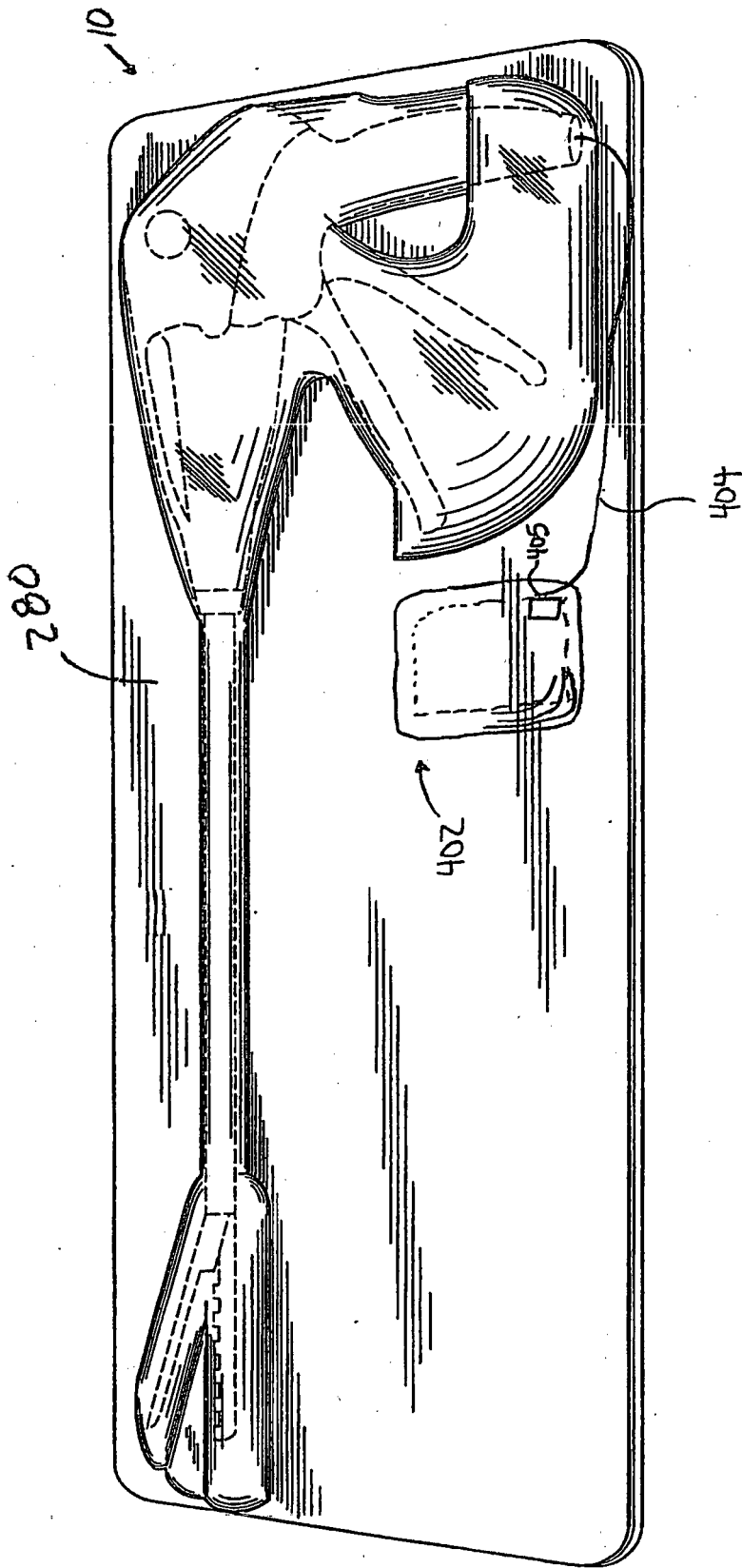


FIG. 16

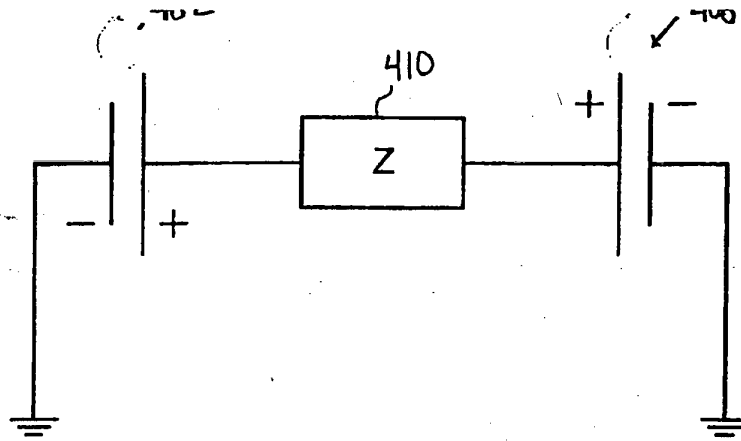


FIG. 17

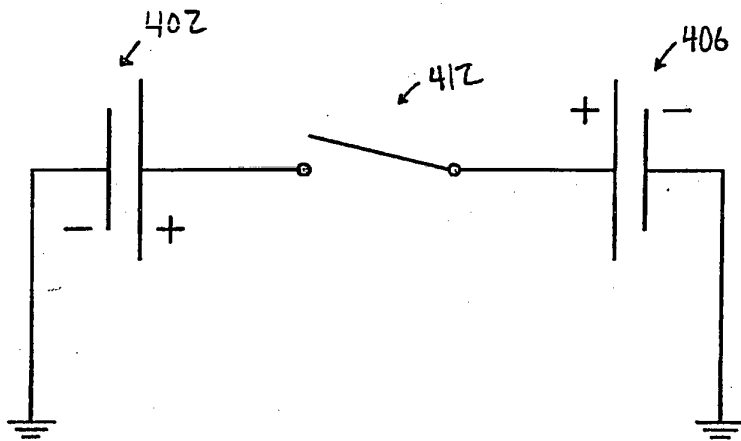


FIG. 18

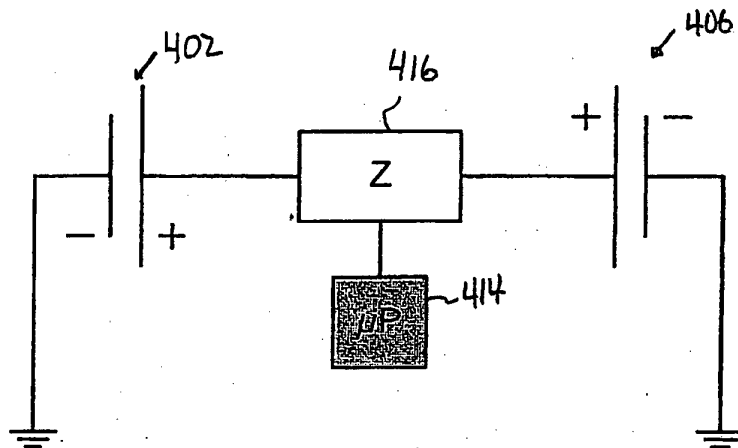


FIG. 19

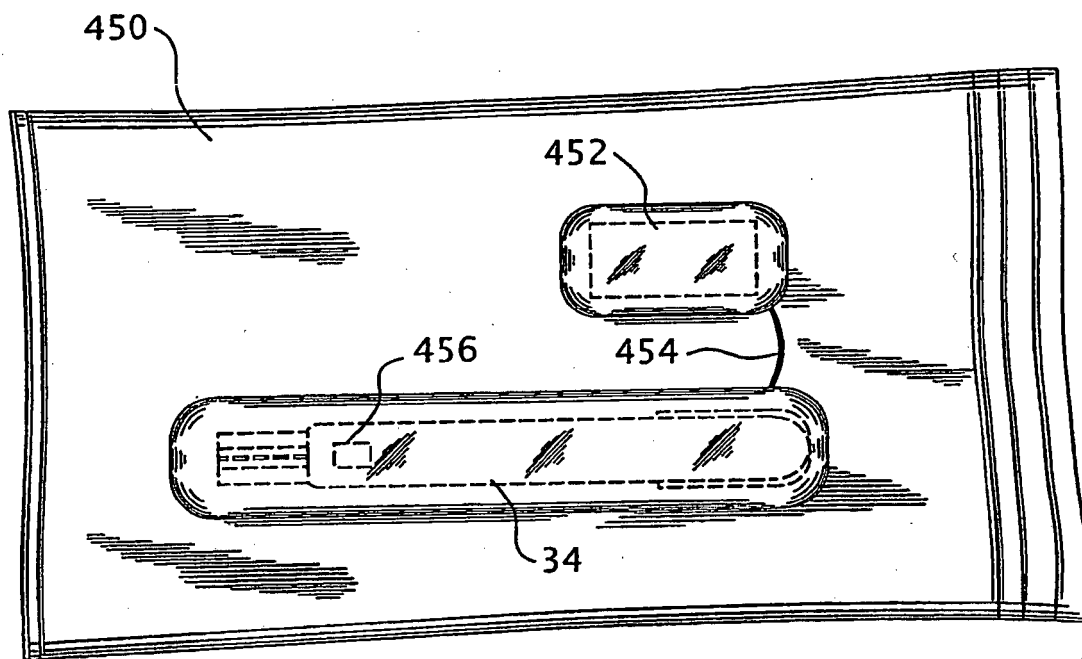


FIG. 20

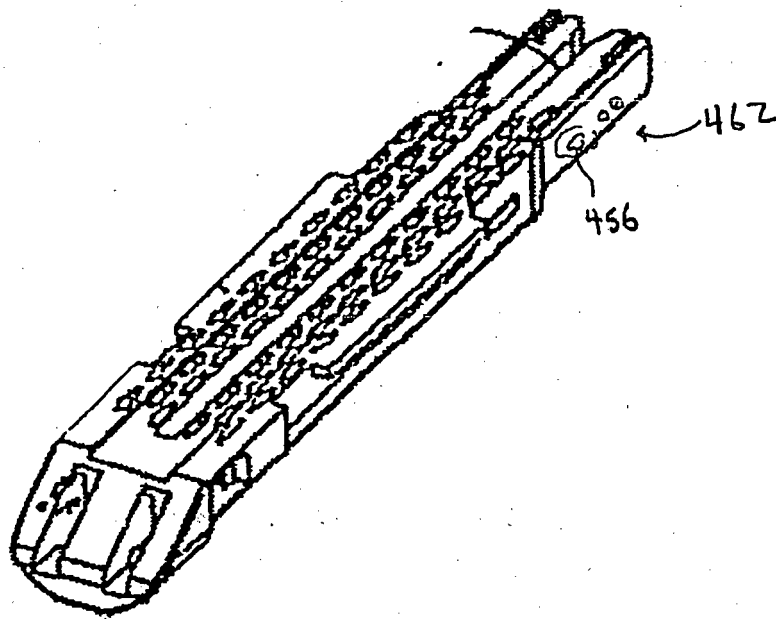


FIG. 21

**REFERENCES CITED IN THE DESCRIPTION**

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专利名称(译)	手术器械具有增强的电池性能		
公开(公告)号	<a href="#">EP1943976B1</a>	公开(公告)日	2014-04-30
申请号	EP2008250099	申请日	2008-01-09
[标]申请(专利权)人(译)	伊西康内外科公司		
申请(专利权)人(译)	爱惜康内镜手术，INC.		
当前申请(专利权)人(译)	爱惜康内镜手术，INC.		
[标]发明人	SHELTON IV FREDERICK E GIORDANO JAMES R SWAYZE JEFFREY S SIEBENALER DOUGLAS J		
发明人	SHELTON IV, FREDERICK E. GIORDANO, JAMES R. SWAYZE, JEFFREY S. SIEBENALER, DOUGLAS J.		
IPC分类号	A61B19/02 A61B17/072		
CPC分类号	A61B17/07207 A61B50/30 A61B90/361 A61B90/98 A61B2017/00022 A61B2017/0003 A61B2017/00362 A61B2017/00473 A61B2017/00734 A61B2017/0688 A61B2017/07271 A61B2034/2051 A61B2090/0811		
优先权	11/651785 2007-01-10 US		
其他公开文献	EP1943976A3 EP1943976A2		
外部链接	<a href="#">Espacenet</a>		

# 摘要(译)

一种组件，包括手术器械的部件，例如内窥镜或腹腔镜器械。该组件可包括包装;包装内的手术器械部件;和包装内的电源。电源可以配置成与手术器械部件电连通。组件还可以包括封装内的辅助电源和电路元件，其中电路元件与电源和辅助电源电连通。

