



(19) **United States**

(12) **Patent Application Publication**  
**KIM et al.**

(10) **Pub. No.: US 2013/0165784 A1**  
(43) **Pub. Date: Jun. 27, 2013**

(54) **PROVIDING MOTION PROFILE INFORMATION OF TARGET OBJECT IN ULTRASOUND SYSTEM**

*A61B 8/14* (2006.01)  
*A61B 8/00* (2006.01)

(52) **U.S. CL.**  
CPC ..... *A61B 8/5246* (2013.01); *A61B 8/488* (2013.01); *A61B 8/145* (2013.01); *A61B 8/463* (2013.01); *A61B 8/5207* (2013.01); *A61B 8/469* (2013.01); *A61B 8/483* (2013.01); *A61B 8/466* (2013.01); *A61B 8/02* (2013.01); *A61B 8/06* (2013.01); *A61B 8/4444* (2013.01); *A61B 8/4488* (2013.01)  
USPC ..... **600/441**

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(21) Appl. No.: **13/728,609**

(22) Filed: **Dec. 27, 2012**

(30) **Foreign Application Priority Data**

Dec. 27, 2011 (KR) ..... 10-2011-0143827

**Publication Classification**

(51) **Int. Cl.**  
*A61B 8/08* (2006.01)  
*A61B 8/06* (2006.01)  
*A61B 8/02* (2006.01)

(57) **ABSTRACT**

There are provided embodiments for providing motion profile information corresponding to a motion of a target object by using vector Doppler. In one embodiment, by way of non-limiting example, an ultrasound system comprises: a processing unit configured to form vector information of a target object based on ultrasound data corresponding to the target object, form a Doppler mode image based on the vector information, and set a first region of interest on the Doppler mode image based on input information of a user, the processing unit being further configured to form motion profile information corresponding to the motion of the target object based on vector information corresponding to the first region of interest.

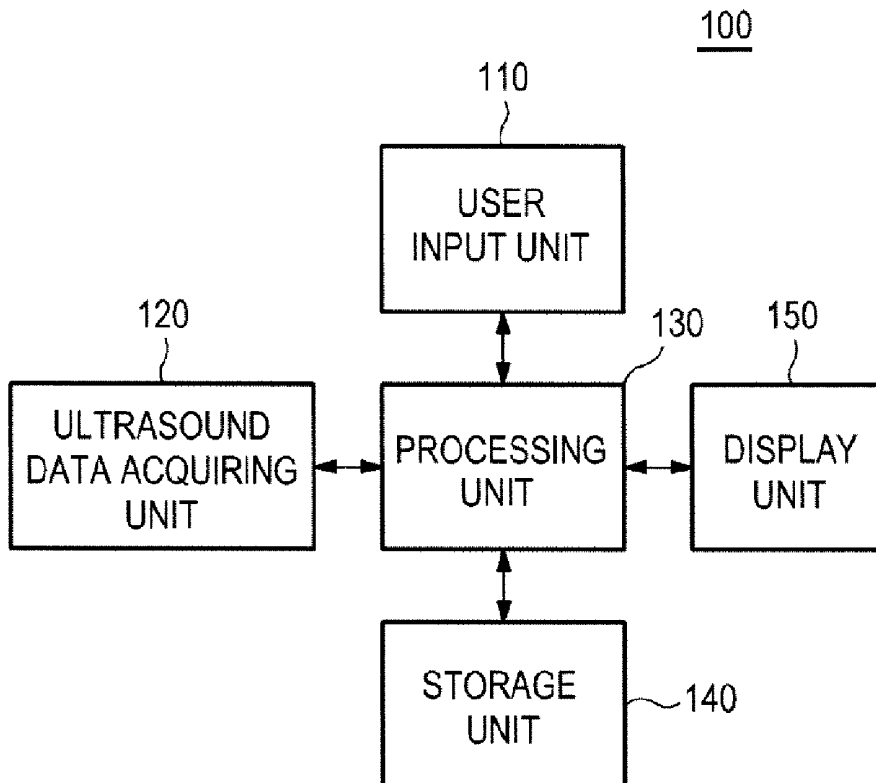


FIG. 1

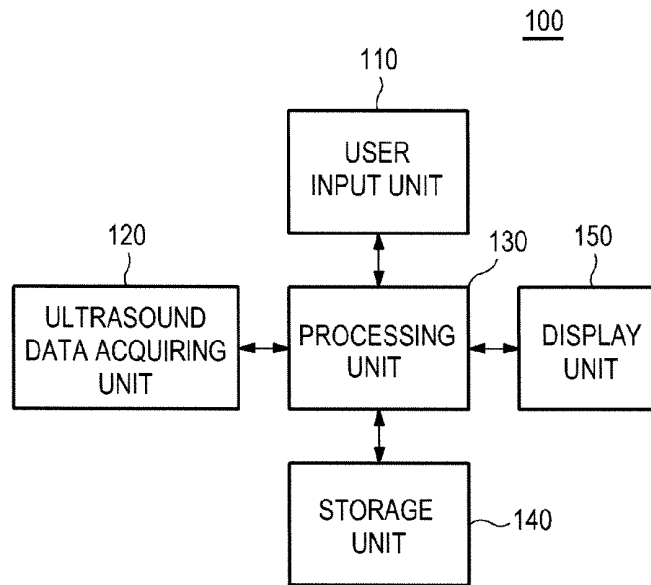


FIG. 11

$S_{1,t}$	$S_{2,t}$	$S_{3,t}$	$S_{4,t}$	$S_{5,t}$	$S_{6,t}$	$S_{7,t}$	$S_{8,t}$	$S_{9,t}$	$S_{10,t}$	$S_{11,t}$	...	$S_{p,t}$
⋮	⋮	⋮	⋮	⋮	⋮	⋮	⋮	⋮	⋮	⋮	⋮	⋮
$S_{1,6}$	$S_{2,6}$	$S_{3,6}$	$S_{4,6}$	$S_{5,6}$	$S_{6,6}$	$S_{7,6}$	$S_{8,6}$	$S_{9,6}$	$S_{10,6}$	$S_{11,6}$	...	$S_{p,6}$
$S_{1,5}$	$S_{2,5}$	$S_{3,5}$	$S_{4,5}$	$S_{5,5}$	$S_{6,5}$	$S_{7,5}$	$S_{8,5}$	$S_{9,5}$	$S_{10,5}$	$S_{11,5}$	...	$S_{p,5}$
$S_{1,4}$	$S_{2,4}$	$S_{3,4}$	$S_{4,4}$	$S_{5,4}$	$S_{6,4}$	$S_{7,4}$	$S_{8,4}$	$S_{9,4}$	$S_{10,4}$	$S_{11,4}$	...	$S_{p,4}$
$S_{1,3}$	$S_{2,3}$	$S_{3,3}$	$S_{4,3}$	$S_{5,3}$	$S_{6,3}$	$S_{7,3}$	$S_{8,3}$	$S_{9,3}$	$S_{10,3}$	$S_{11,3}$	...	$S_{p,3}$
$S_{1,2}$	$S_{2,2}$	$S_{3,2}$	$S_{4,2}$	$S_{5,2}$	$S_{6,2}$	$S_{7,2}$	$S_{8,2}$	$S_{9,2}$	$S_{10,2}$	$S_{11,2}$	...	$S_{p,2}$
$S_{1,1}$	$S_{2,1}$	$S_{3,1}$	$S_{4,1}$	$S_{5,1}$	$S_{6,1}$	$S_{7,1}$	$S_{8,1}$	$S_{9,1}$	$S_{10,1}$	$S_{11,1}$	...	$S_{p,1}$
$CH_1$	$CH_2$	$CH_3$	$CH_4$	$CH_5$	$CH_6$	$CH_7$	$CH_8$	$CH_9$	$CH_{10}$	$CH_{11}$	...	$CH_p$

$P_{1,1}$	$P_{1,2}$	$P_{1,3}$	$P_{1,4}$	$P_{1,5}$	$P_{1,6}$	$P_{1,7}$	$P_{1,8}$	$P_{1,9}$	...	$P_{1,N}$
$P_{2,1}$	$P_{2,2}$	$P_{2,3}$	$P_{2,4}$	$P_{2,5}$	$P_{2,6}$	$P_{2,7}$	$P_{2,8}$	$P_{2,9}$	...	$P_{2,N}$
$P_{3,1}$	$P_{3,2}$	$P_{3,3}$	$P_{3,4}$	$P_{3,5}$	$P_{3,6}$	$P_{3,7}$	$P_{3,8}$	$P_{3,9}$	...	$P_{3,N}$
$P_{4,1}$	$P_{4,2}$	$P_{4,3}$	$P_{4,4}$	$P_{4,5}$	$P_{4,6}$	$P_{4,7}$	$P_{4,8}$	$P_{4,9}$	...	$P_{4,N}$
$P_{5,1}$	$P_{5,2}$	$P_{5,3}$	$P_{5,4}$	$P_{5,5}$	$P_{5,6}$	$P_{5,7}$	$P_{5,8}$	$P_{5,9}$	...	$P_{5,N}$
$P_{6,1}$	$P_{6,2}$	$P_{6,3}$	$P_{6,4}$	$P_{6,5}$	$P_{6,6}$	$P_{6,7}$	$P_{6,8}$	$P_{6,9}$	...	$P_{6,N}$
$P_{7,1}$	$P_{7,2}$	$P_{7,3}$	$P_{7,4}$	$P_{7,5}$	$P_{7,6}$	$P_{7,7}$	$P_{7,8}$	$P_{7,9}$	...	$P_{7,N}$
⋮	⋮	⋮	⋮	⋮	⋮	⋮	⋮	⋮	⋮	⋮
$P_{M,1}$	$P_{M,2}$	$P_{M,3}$	$P_{M,4}$	$P_{M,5}$	$P_{M,6}$	$P_{M,7}$	$P_{M,8}$	$P_{M,9}$	...	$P_{M,N}$

$\swarrow$   $CV_{6,4}$   
 $\swarrow$  UI



FIG. 13

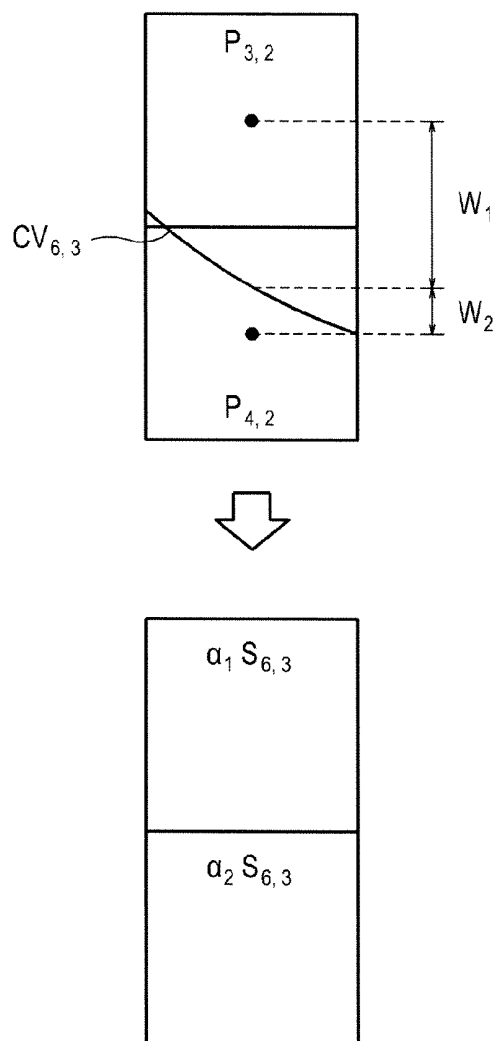


FIG. 14

S <sub>1,t</sub>	S <sub>2,t</sub>	S <sub>3,t</sub>	S <sub>4,t</sub>	S <sub>5,t</sub>	S <sub>6,t</sub>	S <sub>7,t</sub>	S <sub>8,t</sub>	S <sub>9,t</sub>	S <sub>10,t</sub>	S <sub>11,t</sub>	...	S <sub>p,t</sub>
⋮	⋮	⋮	⋮	⋮	⋮	⋮	⋮	⋮	⋮	⋮	⋮	⋮
S <sub>1,6</sub>	S <sub>2,6</sub>	S <sub>3,6</sub>	S <sub>4,6</sub>	S <sub>5,6</sub>	S <sub>6,6</sub>	S <sub>7,6</sub>	S <sub>8,6</sub>	S <sub>9,6</sub>	S <sub>10,6</sub>	S <sub>11,6</sub>	...	S <sub>p,6</sub>
S <sub>1,5</sub>	S <sub>2,5</sub>	S <sub>3,5</sub>	S <sub>4,5</sub>	S <sub>5,5</sub>	S <sub>6,5</sub>	S <sub>7,5</sub>	S <sub>8,5</sub>	S <sub>9,5</sub>	S <sub>10,5</sub>	S <sub>11,5</sub>	...	S <sub>p,5</sub>
S <sub>1,4</sub>	S <sub>2,4</sub>	S <sub>3,4</sub>	S <sub>4,4</sub>	S <sub>5,4</sub>	S <sub>6,4</sub>	S <sub>7,4</sub>	S <sub>8,4</sub>	S <sub>9,4</sub>	S <sub>10,4</sub>	S <sub>11,4</sub>	...	S <sub>p,4</sub>
S <sub>1,3</sub>	S <sub>2,3</sub>	S <sub>3,3</sub>	S <sub>4,3</sub>	S <sub>5,3</sub>	S <sub>6,3</sub>	S <sub>7,3</sub>	S <sub>8,3</sub>	S <sub>9,3</sub>	S <sub>10,3</sub>	S <sub>11,3</sub>	...	S <sub>p,3</sub>
S <sub>1,2</sub>	S <sub>2,2</sub>	S <sub>3,2</sub>	S <sub>4,2</sub>	S <sub>5,2</sub>	S <sub>6,2</sub>	S <sub>7,2</sub>	S <sub>8,2</sub>	S <sub>9,2</sub>	S <sub>10,2</sub>	S <sub>11,2</sub>	...	S <sub>p,2</sub>
S <sub>1,1</sub>	S <sub>2,1</sub>	S <sub>3,1</sub>	S <sub>4,1</sub>	S <sub>5,1</sub>	S <sub>6,1</sub>	S <sub>7,1</sub>	S <sub>8,1</sub>	S <sub>9,1</sub>	S <sub>10,1</sub>	S <sub>11,1</sub>	...	S <sub>p,1</sub>
CH <sub>1</sub>	CH <sub>2</sub>	CH <sub>3</sub>	CH <sub>4</sub>	CH <sub>5</sub>	CH <sub>6</sub>	CH <sub>7</sub>	CH <sub>8</sub>	CH <sub>9</sub>	CH <sub>10</sub>	CH <sub>11</sub>	...	CH <sub>p</sub>

P <sub>1,1</sub>	P <sub>1,2</sub>	P <sub>1,3</sub>	P <sub>1,4</sub>	P <sub>1,5</sub>	P <sub>1,6</sub>	P <sub>1,7</sub>	P <sub>1,8</sub>	P <sub>1,9</sub>	...	P <sub>1,N</sub>
P <sub>2,1</sub>	P <sub>2,2</sub>	P <sub>2,3</sub>	P <sub>2,4</sub>	P <sub>2,5</sub>	P <sub>2,6</sub>	P <sub>2,7</sub>	P <sub>2,8</sub>	P <sub>2,9</sub>	...	P <sub>2,N</sub>
P <sub>3,1</sub>	P <sub>3,2</sub>	P <sub>3,3</sub>	P <sub>3,4</sub>	P <sub>3,5</sub>	P <sub>3,6</sub>	P <sub>3,7</sub>	P <sub>3,8</sub>	P <sub>3,9</sub>	...	P <sub>3,N</sub>
P <sub>4,1</sub>	P <sub>4,2</sub>	P <sub>4,3</sub>	P <sub>4,4</sub>	P <sub>4,5</sub>	P <sub>4,6</sub>	P <sub>4,7</sub>	P <sub>4,8</sub>	P <sub>4,9</sub>	...	P <sub>4,N</sub>
P <sub>5,1</sub>	P <sub>5,2</sub>	P <sub>5,3</sub>	P <sub>5,4</sub>	P <sub>5,5</sub>	P <sub>5,6</sub>	P <sub>5,7</sub>	P <sub>5,8</sub>	P <sub>5,9</sub>	...	P <sub>5,N</sub>
P <sub>6,1</sub>	P <sub>6,2</sub>	P <sub>6,3</sub>	P <sub>6,4</sub>	P <sub>6,5</sub>	P <sub>6,6</sub>	P <sub>6,7</sub>	P <sub>6,8</sub>	P <sub>6,9</sub>	...	P <sub>6,N</sub>
P <sub>7,1</sub>	P <sub>7,2</sub>	P <sub>7,3</sub>	P <sub>7,4</sub>	P <sub>7,5</sub>	P <sub>7,6</sub>	P <sub>7,7</sub>	P <sub>7,8</sub>	P <sub>7,9</sub>	...	P <sub>7,N</sub>
⋮	⋮	⋮	⋮	⋮	⋮	⋮	⋮	⋮	⋮	⋮
P <sub>M,1</sub>	P <sub>M,2</sub>	P <sub>M,3</sub>	P <sub>M,4</sub>	P <sub>M,5</sub>	P <sub>M,6</sub>	P <sub>M,7</sub>	P <sub>M,8</sub>	P <sub>M,9</sub>	...	P <sub>M,N</sub>

UI

FIG. 15

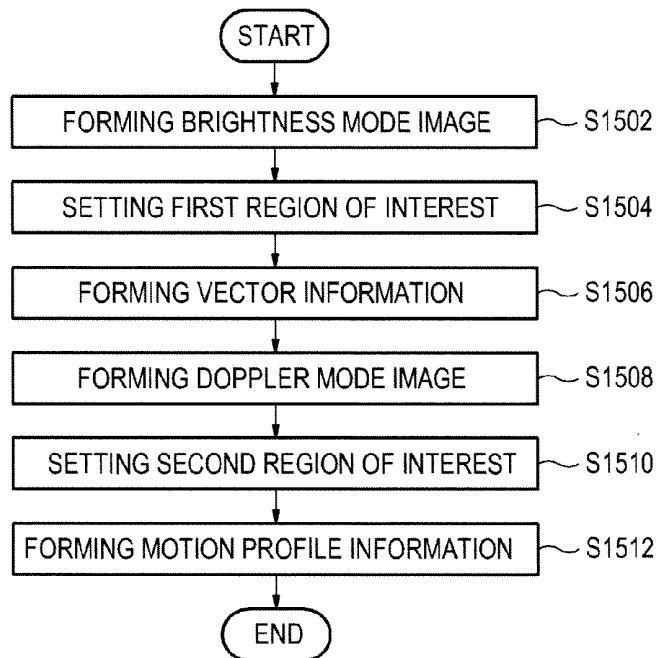


FIG. 16

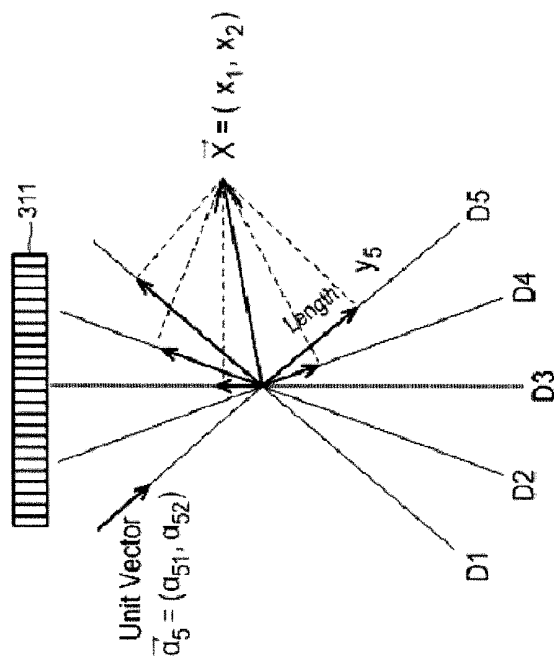
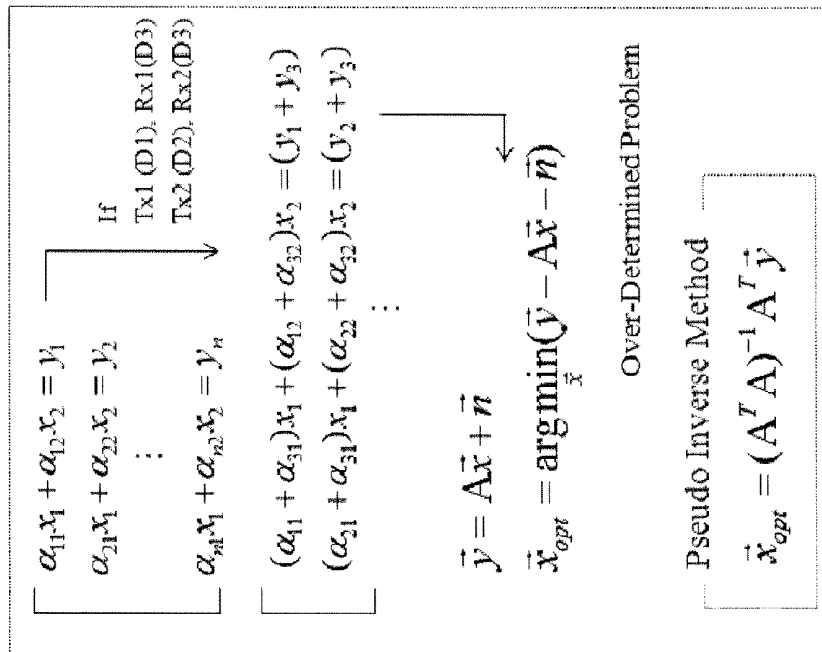


FIG. 17

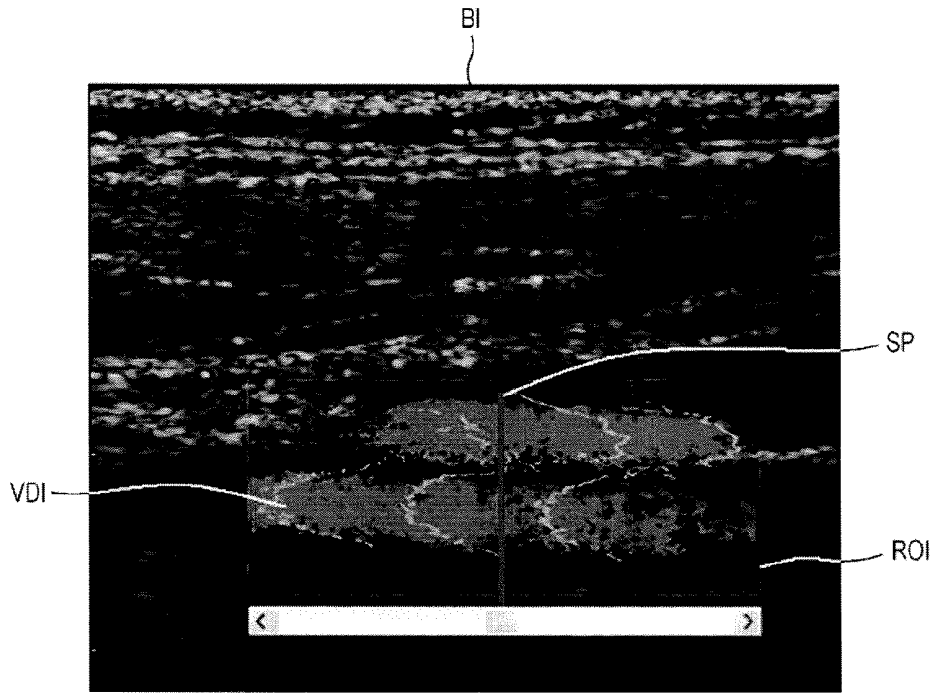


FIG. 18

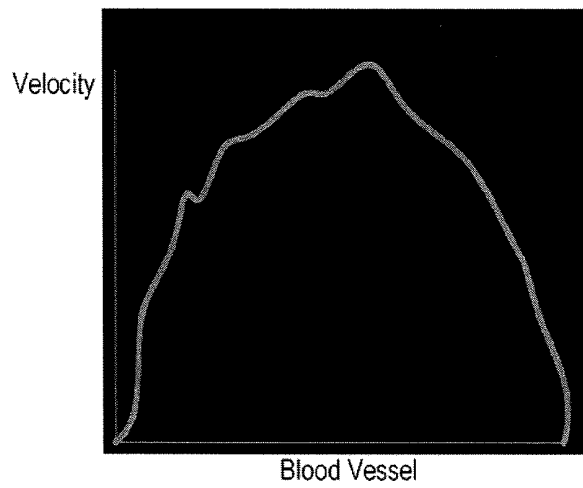


FIG. 19

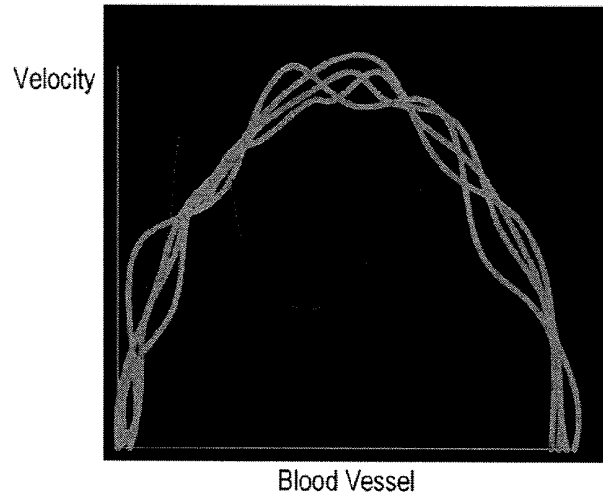


FIG. 20

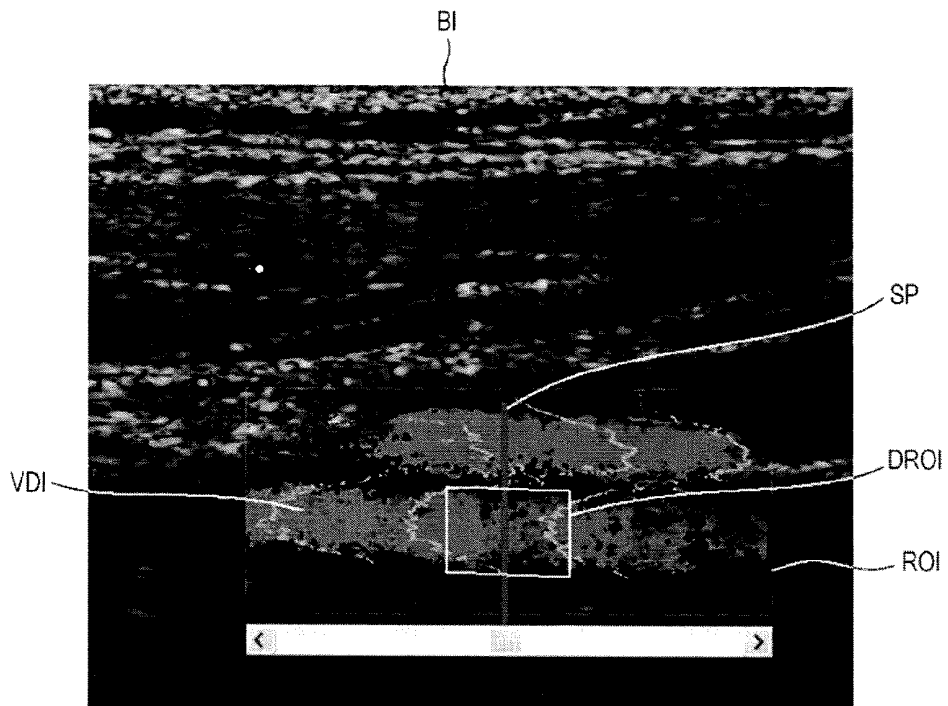


FIG. 21

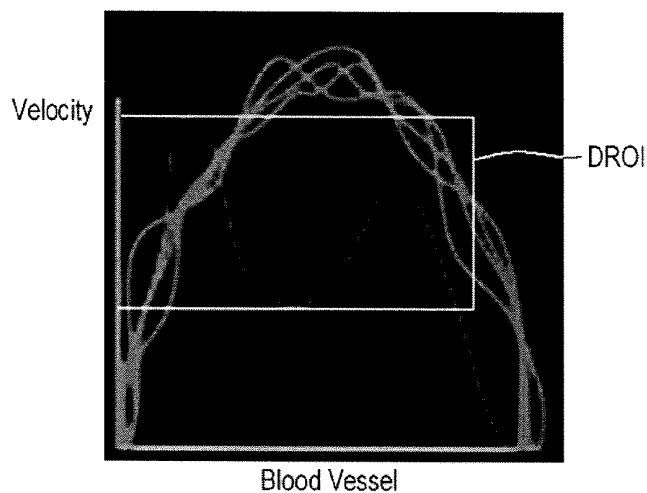


FIG. 22

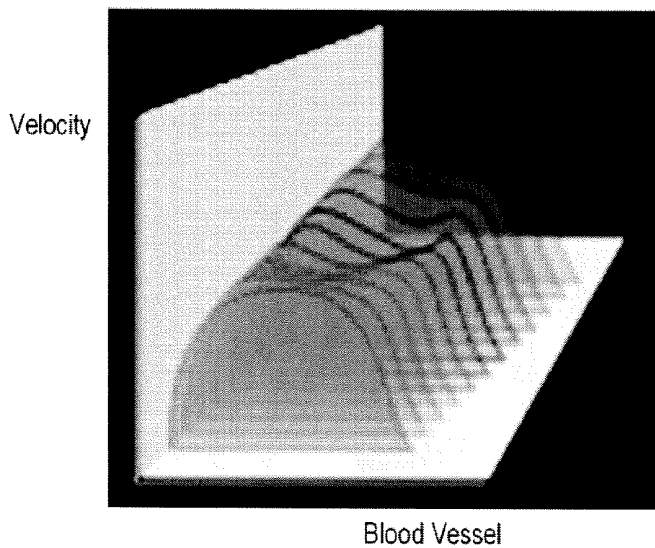


FIG. 23

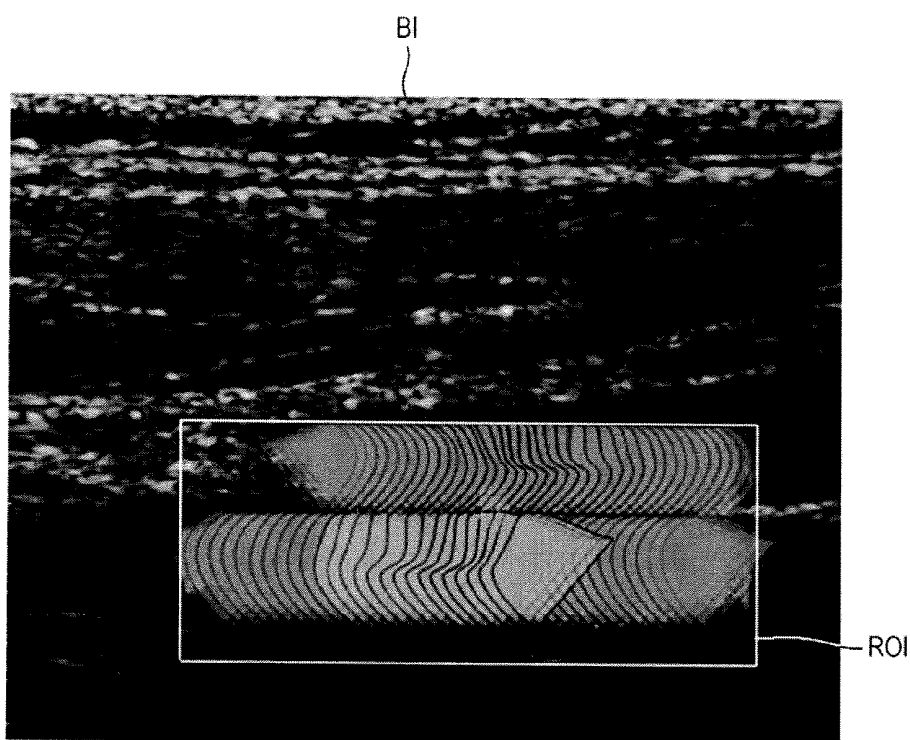


FIG. 2

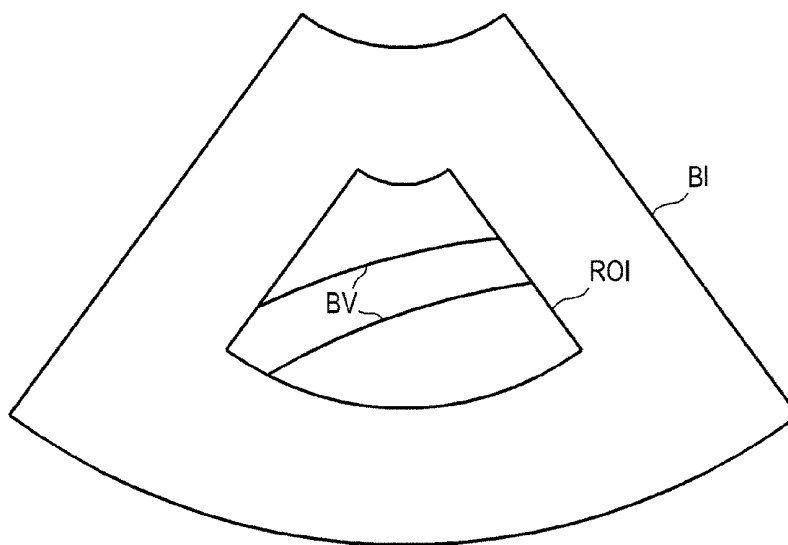
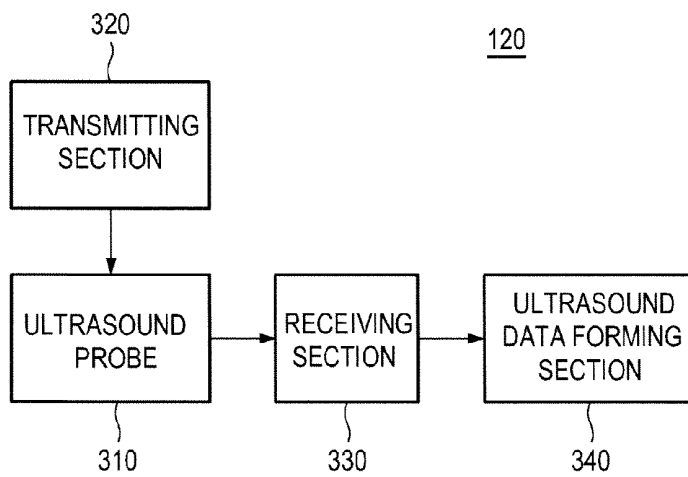


FIG. 3



**PROVIDING MOTION PROFILE  
INFORMATION OF TARGET OBJECT IN  
ULTRASOUND SYSTEM**

CROSS-REFERENCE TO RELATED  
APPLICATIONS

**[0001]** The present application claims priority from Korean Patent Application No. 10-2011-0143827 filed on Dec. 27, 2011, the entire subject matter of which is incorporated herein by reference.

TECHNICAL FIELD

**[0002]** The present disclosure generally relates to ultrasound systems, and more particularly to providing the motion profile information of a target object by using vector Doppler in an ultrasound system.

BACKGROUND

**[0003]** An ultrasound system has become an important and popular diagnostic tool since it has a wide range of applications. Specifically, due to its non-invasive and non-destructive nature, the ultrasound system has been extensively used in the medical profession. Modern high-performance ultrasound systems and techniques are commonly used to produce two-dimensional or three-dimensional ultrasound images of internal features of target objects (e.g., human organs).

**[0004]** The ultrasound system may provide ultrasound images of various modes including a brightness mode image representing reflection coefficients of ultrasound signals (i.e., ultrasound echo signals) reflected from a target object of a living body with a two-dimensional image, a Doppler mode image representing velocity of a moving target object with spectral Doppler by using a Doppler effect, a color Doppler mode image representing velocity of the moving target object with colors by using the Doppler effect, an elastic image representing mechanical characteristics of tissues before and after applying compression thereto and the like.

**[0005]** The ultrasound system may transmit the ultrasound signals to the living body and receive the ultrasound echo signals from the living body to form Doppler signals corresponding to a region of interest, which is set on the brightness mode image. The ultrasound system may further form the color Doppler mode image representing the velocity of the moving target object with colors based on the Doppler signals. In particular, the color Doppler image may represent the motion of the target object (e.g., blood flow) with the colors. The color Doppler image may be used to diagnose diseases of blood vessels, heart and the like. However, it is difficult to represent an accurate motion of the target object (e.g., blood flow) since the respective colors indicated by a motion value is a function of the velocity of the target object, which moves forward in a transmission direction of the ultrasound signals and moves backward in the transmission direction of the ultrasound signals.

**[0006]** To resolve this problem, a vector Doppler method capable of obtaining the velocity and direction of the blood flow is used. A cross beam-based method of the vector Doppler method may acquire velocity magnitude components from at least two different directions, and combine the velocity magnitude components to detect vector information having a two-dimensional or three-dimensional direction information and a magnitude information.

SUMMARY

**[0007]** There are provided embodiments for providing the motion profile information corresponding to the motion of a target object by using vector Doppler.

**[0008]** In one embodiment, by way of non-limiting example, an ultrasound system comprises: a processing unit configured to form vector information of a target object based on ultrasound data corresponding to the target object, form a Doppler mode image based on the vector information, and set a first region of interest on the Doppler mode image based on input information of a user, the processing unit being further configured to form motion profile information corresponding to the motion of the target object based on vector information corresponding to the first region of interest.

**[0009]** In another embodiment, there is provided a method of providing motion profile information, comprising: a) forming vector information of a target object based on ultrasound data corresponding to the target object; b) forming a Doppler mode image based on the vector information; c) setting a first region of interest on the Doppler mode image based on input information of a user; and d) forming motion profile information corresponding to motion of the target object based on the vector information corresponding to the first region of interest.

**[0010]** The Summary is provided to introduce a selection of concepts in a simplified form that are further described below in the Detailed Description. This Summary is not intended to identify key or essential features of the claimed subject matter, nor is it intended to be used in determining the scope of the claimed subject matter.

BRIEF DESCRIPTION OF THE DRAWINGS

**[0011]** FIG. 1 is a block diagram showing an illustrative embodiment of an ultrasound system.

**[0012]** FIG. 2 is a schematic diagram showing an example of a brightness mode image and a first region of interest.

**[0013]** FIG. 3 is a block diagram showing an illustrative embodiment of an ultrasound data acquiring unit.

**[0014]** FIGS. 4 to 7 are schematic diagrams showing examples of transmission directions and reception directions.

**[0015]** FIG. 8 is a schematic diagram showing an example of sampling data and pixels of an ultrasound image.

**[0016]** FIGS. 9 to 12 are schematic diagrams showing examples of performing a reception beam-forming.

**[0017]** FIG. 13 is a schematic diagram showing an example of setting weights.

**[0018]** FIG. 14 is a schematic diagram showing an example of setting a sampling data set.

**[0019]** FIG. 15 is a flow chart showing a process of forming motion profile information.

**[0020]** FIG. 16 is a schematic diagram showing an example of the transmission directions, the reception directions, the vector information and an over-determined problem.

**[0021]** FIG. 17 is a schematic diagram showing an example of a second region of interest.

**[0022]** FIGS. 18 and 19 are schematic diagrams showing examples of the motion profile information.

**[0023]** FIGS. 20 and 21 are schematic diagrams showing examples of a third region of interest.

**[0024]** FIGS. 22 and 23 are schematic diagrams showing examples of three-dimensional motion profile information.

## DETAILED DESCRIPTION

[0025] A detailed description may be provided with reference to the accompanying drawings. One of ordinary skill in the art may realize that the following description is illustrative only and is not in any way limiting. Other embodiments of the present invention may readily suggest themselves to such skilled persons having the benefit of this disclosure.

[0026] Referring to FIG. 1, an ultrasound system 100 in accordance with an illustrative embodiment is shown. As depicted therein, the ultrasound system 100 may include a user input unit 110.

[0027] The user input unit 110 may be configured to receive input information from a user. In one embodiment, the input information may include first input information for setting a first region of interest ROI on a brightness mode image BI, as shown in FIG. 2. The first region of interest ROI may include a color box for obtaining a Doppler mode image. The Doppler mode image may include a vector Doppler image or a color Doppler image. However, it should be noted herein that the Doppler mode image may not be limited thereto. The input information may further include second input information for setting a second region of interest on the Doppler mode image. The second region of interest may be a region of interest for obtaining profile information (hereinafter referred to as "motion profile information") corresponding to change of vector information (i.e., motion of target object) with time. The input information may also include third input information for setting a third region of interest on the Doppler mode image or the motion profile information. The third region of interest will be described below in detail. In FIG. 2, the reference numeral BV represents a blood vessel. The user input unit 110 may include a control panel, a track ball, a touch screen, a mouse, a keyboard and the like.

[0028] The ultrasound system 100 may further include an ultrasound data acquiring unit 120. The ultrasound data acquiring unit 120 may be configured to transmit ultrasound signals to a living body. The living body may include moving target objects (e.g., blood vessel, heart, blood flow, etc). The ultrasound data acquiring unit 120 may be further configured to receive ultrasound signals (i.e., ultrasound echo signals) from the living body to acquire ultrasound data corresponding to an ultrasound image.

[0029] FIG. 3 is a block diagram showing an illustrative embodiment of the ultrasound data acquiring unit. Referring to FIG. 3, the ultrasound data acquiring unit 120 may include an ultrasound probe 310.

[0030] The ultrasound probe 310 may include a plurality of elements 311 (see FIG. 4) for reciprocally converting between ultrasound signals and electrical signals. The ultrasound probe 310 may be configured to transmit the ultrasound signals to the living body. The ultrasound signals transmitted from the ultrasound probe 310 may be plane wave signals that the ultrasound signals are not focused at a focusing point or focused signals that the ultrasound signals are focused at the focusing point. However, it should be noted herein that the ultrasound signals may not be limited thereto. The ultrasound probe 310 may be further configured to receive the ultrasound echo signals from the living body to output electrical signals (hereinafter referred to as "reception signals"). The reception signals may be analog signals. The ultrasound probe 310 may include a convex probe, a linear probe, a phased array probe and the like.

[0031] The ultrasound data acquiring unit 120 may further include a transmitting section 320. The transmitting section

320 may be configured to control the transmission of the ultrasound signals. The transmitting section 320 may be further configured to generate electrical signals (hereinafter referred to as "transmission signals") in consideration of the elements 311.

[0032] In one embodiment, the transmitting section 320 may be configured to generate transmission signals (hereinafter referred to as "brightness mode transmission signals") for obtaining the brightness mode image BI in consideration of the elements 311. Thus, the ultrasound probe 310 may be configured to convert the brightness mode transmission signals provided from the transmitting section 320 into the ultrasound signals, transmit the ultrasound signals to the living body, and receive the ultrasound echo signals from the living body to output reception signals (hereinafter referred to as "brightness mode reception signals").

[0033] The transmitting section 320 may be further configured to generate transmission signals (hereinafter referred to as "Doppler mode transmission signals") corresponding to an ensemble number in consideration of the elements 311 and at least one transmission direction of the ultrasound signals (i.e., transmission beam). Thus, the ultrasound probe 310 may be configured to convert the Doppler mode transmission signals provided from the transmitting section 320 into the ultrasound signals, transmit the ultrasound signals to the living body in the at least one transmission signals, and receive the ultrasound echo signals from the living body to output reception signals (hereinafter referred to as "Doppler mode reception signals"). The ensemble number may represent the number of transmitting and receiving the ultrasound signals.

[0034] As one example, the transmitting section 320 may be configured to generate the Doppler mode transmission signals corresponding to the ensemble number in consideration of a transmission direction Tx and the elements 311, as shown in FIG. 4. The transmission direction may be one of a direction (i.e., 0 degree) perpendicular to a longitudinal direction of the elements 311 to a maximum steering direction of the transmission beam.

[0035] As another example, the transmitting section 320 may be configured to generate first Doppler mode transmission signals corresponding to the ensemble number in consideration of a first transmission direction Tx<sub>1</sub> and the elements 311, as shown in FIG. 5. Thus, the ultrasound probe 310 may be configured to convert the first Doppler mode transmission signals provided from the transmitting section 320 into the ultrasound signals, transmit the ultrasound signals to the living body in the first transmission direction Tx<sub>1</sub>, and receive the ultrasound echo signals from the living body to output first Doppler mode reception signals. The transmitting section 320 may be further configured to generate second Doppler mode transmission signals corresponding to the ensemble number in consideration of a second transmission direction Tx<sub>2</sub> and the elements 311, as shown in FIG. 5. Thus, the ultrasound probe 310 may be configured to convert the second Doppler mode transmission signals provided from the transmitting section 320 into the ultrasound signals, transmit the ultrasound signals to the living body in the second transmission direction Tx<sub>2</sub>, and receive the ultrasound echo signals from the living body to output second Doppler mode reception signals. In FIG. 5, the reference numeral PRI represents a pulse repeat interval.

[0036] In another embodiment, the transmitting section 320 may be configured to generate the brightness mode transmission signals for obtaining the brightness mode image BI in

consideration of the elements 311. Thus, the ultrasound probe 310 may be configured to convert the brightness mode transmission signals provided from the transmitting section 320 into the ultrasound signals, transmit the ultrasound signals to the living body, and receive the ultrasound echo signals from the living body to output the brightness mode reception signals.

[0037] The transmitting section 320 may be further configured to generate the Doppler mode transmission signals corresponding to the ensemble number in consideration of the at least one transmission direction and the elements 311. Thus, the ultrasound probe 310 may be configured to convert the Doppler mode transmission signals provided from the transmitting section 320 into the ultrasound signals, transmit the ultrasound signals to the living body, and receive the ultrasound echo signals from the living body to output the Doppler mode reception signals. The ultrasound signals may be transmitted in an interleaved transmission scheme. The interleaved transmission scheme will be described below in detail.

[0038] For example, the transmitting section 320 may be configured to generate the first Doppler mode transmission signals in consideration of the first transmission direction  $Tx_1$  and the elements 311, as shown in FIG. 6. Thus, the ultrasound probe 310 may be configured to convert the first Doppler mode transmission signals provided from the transmitting section 320 into the ultrasound signals, and transmit the ultrasound signals to the living body in the first transmission direction  $Tx_1$ . The transmitting section 320 may be further configured to generate the second Doppler mode transmission signals in consideration of the second transmission direction  $Tx_2$  and the elements 311, as shown in FIG. 6. Thus, the ultrasound probe 310 may be configured to convert the second Doppler mode transmission signals provided from the transmitting section 320 into the ultrasound signals, and transmit the ultrasound signals to the living body in the second transmission direction  $Tx_2$ . The ultrasound probe 310 may be further configured to receive the ultrasound echo signals (i.e., ultrasound echo signals corresponding to first Doppler mode transmission signals) from the living body to output the first Doppler mode reception signals. The ultrasound probe 310 may be further configured to receive the ultrasound echo signals (i.e., ultrasound echo signals corresponding to second Doppler mode transmission signals) from the living body to output the second Doppler mode reception signals.

[0039] Thereafter, the transmitting section 320 may be configured to generate the first Doppler mode transmission signals based on the pulse repeat interval, as shown in FIG. 6. Thus, the ultrasound probe 310 may be configured to convert the first Doppler mode transmission signals provided from the transmitting section 320 into the ultrasound signals, and transmit the ultrasound signals to the living body in the first transmission direction  $Tx_1$ . Then, the transmitting section 320 may be further configured to generate the second Doppler mode transmission signals based on the pulse repeat interval, as shown in FIG. 6. Accordingly, the ultrasound probe 310 may be configured to convert the second Doppler mode transmission signals provided from the transmitting section 320 into the ultrasound signals, and transmit the ultrasound signals to the living body in the second transmission direction  $Tx_2$ . The ultrasound probe 310 may be further configured to receive the ultrasound echo signals (i.e., ultrasound echo signals corresponding to first Doppler mode transmission signals) from the living body to output the first Doppler mode

reception signals. The ultrasound probe 310 may be further configured to receive the ultrasound echo signals (i.e., ultrasound echo signals corresponding to second Doppler mode transmission signals) from the living body to output the second Doppler mode reception signals.

[0040] As described above, the transmitting section 320 may be configured to generate the first Doppler mode transmission signals and the second Doppler mode transmission signals corresponding to the ensemble number.

[0041] In yet another embodiment, the transmitting section 320 may be configured to generate the brightness mode transmission signals for obtaining the brightness mode image BI in consideration of the elements 311. Thus, the ultrasound probe 310 may be configured to convert the brightness mode transmission signals provided from the transmitting section 320 into the ultrasound signals, transmit the ultrasound signals to the living body, and receive the ultrasound echo signals from the living body to output the brightness mode reception signals.

[0042] The transmitting section 320 may be further configured to generate the Doppler mode transmission signals corresponding to the ensemble number in consideration of the at least one transmission direction and the elements 311. Thus, the ultrasound probe 310 may be configured to convert the Doppler mode transmission signals provided from the transmitting section 320 into the ultrasound signals, transmit the ultrasound signals to the living body in the at least one transmission direction, and receive the ultrasound echo signals from the living body to output the Doppler mode reception signals. The ultrasound signals may be transmitted according to the pulse repeat interval.

[0043] For example, the transmitting section 320 may be configured to generate the first Doppler mode transmission signals in consideration of the first transmission direction  $Tx_1$  and the elements 311 based on the pulse repeat interval, as shown in FIG. 7. Thus, the ultrasound probe 310 may be configured to convert the first Doppler mode transmission signals provided from the transmitting section 320 into the ultrasound signals, transmit the ultrasound signals to living body in the first transmission direction  $Tx_1$ , and receive the ultrasound echo signals from the living body to output the first Doppler mode reception signals. The transmitting section 320 may be further configured to generate the second Doppler mode transmission signals in consideration of the second transmission direction  $Tx_2$  and the elements 311 based on the pulse repeat interval, as shown in FIG. 7. Thus, the ultrasound probe 310 may be configured to convert the second Doppler mode transmission signals provided from the transmitting section 320 into the ultrasound signals, transmit the ultrasound signals to the living body in the second transmission direction  $Tx_2$ , and receive the ultrasound echo signals from the living body to output the second Doppler mode reception signals.

[0044] As described above, the transmitting section 320 may be configured to generate the first Doppler mode transmission signals and the second Doppler mode transmission signals corresponding to the ensemble number based on the pulse repeat interval.

[0045] Referring back to FIG. 3, the ultrasound data acquiring unit 120 may further include a receiving section 330. The receiving section 330 may be configured to perform an analog-digital conversion upon the reception signals provided from the ultrasound probe 310 to form sampling data. The receiving section 330 may be further configured to perform a

reception beam-forming upon the sampling data in consideration of the elements 311 to form reception-focused data. The reception beam-forming will be described below in detail.

**[0046]** In one embodiment, the receiving section 330 may be configured to perform the analog-digital conversion upon the brightness mode reception signals provided from the ultrasound probe 310 to form sampling data (hereinafter, referred to as “brightness mode sampling data”). The receiving section 330 may be further configured to perform the reception beam-forming upon the brightness mode sampling data to form reception-focused data (hereinafter referred to as “brightness mode reception-focused data”).

**[0047]** The receiving section 330 may be further configured to perform the analog-digital conversion upon the Doppler mode reception signals provided from the ultrasound probe 310 to form sampling data (hereinafter referred to as “Doppler mode sampling data”). The receiving section 330 may be further configured to perform the reception beam-forming upon the Doppler mode sampling data to form reception-focused data (hereinafter referred to as “Doppler mode reception-focused data”) corresponding to at least one reception direction of the ultrasound echo signals (i.e., reception beam).

**[0048]** As one example, the receiving section 330 may be configured to perform the analog-digital conversion upon the Doppler mode reception signals provided from the ultrasound probe 310 to form the Doppler mode sampling data. The receiving section 330 may be further configured to perform the reception beam-forming upon the Doppler mode sampling data to form first Doppler mode reception-focused data corresponding to a first reception direction  $Rx_1$  and second Doppler mode reception-focused data corresponding to a second reception direction  $Rx_2$ , as shown in FIG. 4.

**[0049]** As another example, the receiving section 330 may be configured to perform the analog-digital conversion upon the first Doppler mode reception signals provided from the ultrasound probe 310 to form first Doppler mode sampling data corresponding to the first transmission direction  $Tx_1$ , as shown in FIG. 5. The receiving section 330 may be further configured to perform the reception beam-forming upon the first Doppler mode sampling data to form the first Doppler mode reception-focused data corresponding to the first reception direction  $Rx_1$ . The receiving section 330 may be also configured to perform the analog-digital conversion upon the second Doppler mode reception signals provided from the ultrasound probe 310 to form second Doppler mode sampling data corresponding to the second transmission direction  $Tx_2$ , as shown in FIG. 5. The receiving section 330 may be further configured to perform the reception beam-forming upon the second Doppler mode sampling data to form the second Doppler mode reception-focused data corresponding to the second reception direction  $Rx_2$ . If the reception direction is perpendicular to the elements 311 of the ultrasound probe 310, then a maximum aperture size may be used.

**[0050]** The reception beam-forming may be described with reference to the accompanying drawings.

**[0051]** In one embodiment, the receiving section 330 may be configured to perform the analog-digital conversion upon the reception signals provided through a plurality of channels  $CH_k$ , wherein  $1 \leq k \leq N$ , from the ultrasound probe 310 to form sampling data  $S_{i,j}$ , wherein the  $i$  and  $j$  are a positive integer, as shown in FIG. 8. The sampling data  $S_{i,j}$  may be stored in a storage unit 140. The receiving section 330 may be further configured to detect pixels corresponding to the sampling data based on positions of the elements 311 and posi-

tions (orientation) of pixels of the ultrasound image UI with respect to the elements 311. That is, the receiving section 330 may select the pixels, which the respective sampling data are used as pixel data thereof, during the reception beam-forming based on the positions of the elements 311 and the orientation of the respective pixels of the ultrasound image UI with respect to the elements 311. The receiving section 330 may be configured to cumulatively assign the sampling data corresponding to the selected pixels as the pixel data.

**[0052]** For example, the receiving section 330 may be configured to set a curve (hereinafter referred to as “reception beam-forming curve”)  $CV_{6,3}$  for selecting pixels, which the sampling data  $S_{6,3}$  are used as the pixel data thereof, during the reception beam-forming based on the positions of the elements 311 and the orientation of the respective pixels of the ultrasound image UI with respect to the elements 311, as shown in FIG. 9. The receiving section 330 may be further configured to detect the pixels  $P_{3,1}, P_{3,2}, P_{4,2}, P_{4,3}, P_{4,4}, P_{4,5}, P_{4,6}, P_{4,7}, P_{4,8}, P_{4,9}, \dots, P_{3,N}$  corresponding to the reception beam-forming curve  $CV_{6,3}$  from the pixels  $P_{a,b}$  of the ultrasound image UI, wherein  $1 \leq a \leq M, 1 \leq b \leq N$ . That is, the receiving section 330 may select the pixels  $P_{3,1}, P_{3,2}, P_{4,2}, P_{4,3}, P_{4,4}, P_{4,5}, P_{4,6}, P_{4,7}, P_{4,8}, P_{4,9}, \dots, P_{3,N}$  on which the reception beam-forming curve  $CV_{6,3}$  passes among the pixels  $P_{a,b}$  of the ultrasound image UI. The receiving section 330 may be also configured to assign the sampling data  $S_{6,3}$  to the selected pixels  $P_{3,1}, P_{3,2}, P_{4,2}, P_{4,3}, P_{4,4}, P_{4,5}, P_{4,6}, P_{4,7}, P_{4,8}, P_{4,9}, \dots, P_{3,N}$ , as shown in FIG. 10.

**[0053]** Thereafter, the receiving section 330 may be configured to set a reception beam-forming curve  $CV_{6,4}$  for selecting pixels, which the sampling data  $S_{6,4}$  are used as the pixel data thereof, during the reception beam-forming based on the positions of the elements 311 and the orientation of the respective pixels of the ultrasound image UI with respect to the elements 311, as shown in FIG. 11. The receiving section 330 may be further configured to detect the pixels  $P_{2,1}, P_{3,1}, P_{3,2}, P_{4,2}, P_{4,3}, P_{4,4}, P_{5,4}, P_{5,5}, P_{5,6}, P_{5,7}, P_{5,8}, P_{4,9}, P_{5,9}, \dots, P_{4,N}, P_{3,N}$  corresponding to the reception beam-forming curve  $CV_{6,4}$  from the pixels  $P_{a,b}$  of the ultrasound image UI. That is, the receiving section 330 may select the pixels  $P_{2,1}, P_{3,1}, P_{3,2}, P_{4,2}, P_{4,3}, P_{4,4}, P_{5,4}, P_{5,5}, P_{5,6}, P_{5,7}, P_{5,8}, P_{4,9}, P_{5,9}, \dots, P_{4,N}, P_{3,N}$  on which the reception beam-forming curve  $CV_{6,4}$  passes among the pixels  $P_{a,b}$  of the ultrasound image UI. The receiving section 330 may be additionally configured to assign the sampling data  $S_{6,4}$  to the selected pixels  $P_{2,1}, P_{3,1}, P_{3,2}, P_{4,2}, P_{4,3}, P_{4,4}, P_{5,4}, P_{5,5}, P_{5,6}, P_{5,7}, P_{5,8}, P_{4,9}, P_{5,9}, \dots, P_{4,N}, P_{3,N}$ , as shown in FIG. 12. In this way, the respective sampling data, which are used as the pixel data, may be cumulatively assigned to the pixels as the pixel data.

**[0054]** The receiving section 330 may be configured to perform the reception beam-forming (i.e., summing) upon the sampling data, which are cumulatively assigned to the respective pixels  $P_{a,b}$  of the ultrasound image UI to form the reception-focused data.

**[0055]** In another embodiment, the receiving section 330 may be configured to perform the analog-digital conversion upon the reception signals provided through the plurality of channels  $CH_k$  from the ultrasound probe 310 to form the sampling data  $S_{i,j}$ , as shown in FIG. 8. The sampling data  $S_{i,j}$  may be stored in the storage unit 140. The receiving section 330 may be further configured to detect pixels corresponding to the sampling data based on the positions of the elements 311 and the positions (orientation) of the pixels of the ultrasound image UI with respect to the elements 311. That is, the

receiving section 330 may select the pixels, which the respective sampling data are used as the pixel data thereof, during the reception beam-forming based on the positions of the elements 311 and the orientation of the respective pixels of the ultrasound image UI with respect to the elements 311. The receiving section 330 may be configured to cumulatively assign the sampling data corresponding to the selected pixels as the pixel data. The receiving section 330 may be further configured to determine pixels existing in the same column among the selected pixels. The receiving section 330 may be also configured to set weights corresponding to the respective determined pixels. The receiving section 330 may be additionally configured to apply the weights to the sampling data of the respective pixels.

[0056] For example, the receiving section 330 may be configured to set the reception beam-forming curve  $CV_{6,3}$  for selecting pixels, which the sampling data  $S_{6,3}$  are used as the pixel data thereof, during the reception beam-forming based on the positions of the elements 311 and the orientation of the respective pixels of the ultrasound image UI with respect to the elements 311, as shown in FIG. 9. The receiving section 330 may be further configured to detect the pixels  $P_{3,1}, P_{3,2}, P_{4,2}, P_{4,3}, P_{4,4}, P_{4,5}, P_{4,6}, P_{4,7}, P_{4,8}, P_{4,9}, \dots, P_{3,N}$  corresponding to the reception beam-forming curve  $CV_{6,3}$  from the pixels  $P_{a,b}$  of the ultrasound image UI, wherein  $1 \leq a \leq M$ ,  $1 \leq b \leq N$ . That is, the receiving section 330 may select the pixels  $P_{3,1}, P_{3,2}, P_{4,2}, P_{4,3}, P_{4,4}, P_{4,5}, P_{4,6}, P_{4,7}, P_{4,8}, P_{4,9}, \dots, P_{3,N}$  on which the reception beam-forming curve  $CV_{6,3}$  passes among the pixels  $P_{a,b}$  of the ultrasound image UI. The receiving section 330 may be also configured to assign the sampling data  $S_{6,3}$  to the selected pixels  $P_{3,1}, P_{3,2}, P_{4,2}, P_{4,3}, P_{4,4}, P_{4,5}, P_{4,6}, P_{4,7}, P_{4,8}, P_{4,9}, \dots, P_{3,N}$  as shown in FIG. 10. The receiving section 330 may be further configured to determine pixels  $P_{3,2}$  and  $P_{4,2}$ , which exist in the same column among the selected pixels  $P_{3,1}, P_{3,2}, P_{4,2}, P_{4,3}, P_{4,4}, P_{4,5}, P_{4,6}, P_{4,7}, P_{4,8}, P_{4,9}, \dots, P_{3,N}$ . The receiving section 330 may be further configured to calculate a distance  $W_1$  from a center of the determined pixel  $P_{3,2}$  to the reception beam-forming curve  $CV_{6,3}$  and a distance  $W_2$  from a center of the determined pixel  $P_{4,2}$  to the reception beam-forming curve  $CV_{6,3}$ , as shown in FIG. 13. The receiving section 330 may be additionally configured to set a first weight  $\alpha_1$  corresponding to the pixel  $P_{3,2}$  based on the distance  $W_1$  and a second weight  $\alpha_2$  corresponding to the pixel  $P_{4,2}$  based on the distance  $W_2$ . The first weight  $\alpha_1$  and the second weight  $\alpha_2$  may be set to be in proportional to or in inverse proportional to the calculated distances. The receiving section 330 may be further configured to apply the first weight  $\alpha_1$  to the sampling data  $S_{6,3}$  assigned to the pixel  $P_{3,2}$  and to apply the second weight  $\alpha_2$  to the sampling data  $S_{6,3}$  assigned to the pixel  $P_{4,2}$ . The receiving section 330 may be configured to perform the above process upon the remaining sampling data.

[0057] The receiving section 330 may be configured to perform the reception beam-forming upon the sampling data, which are cumulatively assigned to the respective pixels  $P_{a,b}$  of the ultrasound image UI to form the reception-focused data.

[0058] In yet another embodiment, the receiving section 330 may be configured to perform the analog-digital conversion upon the reception signals provided through the plurality of channels  $CH_k$  from the ultrasound probe 310 to form the sampling data  $S_{i,j}$ , as shown in FIG. 8. The sampling data  $S_{i,j}$  may be stored in the storage unit 140. The receiving section 330 may be further configured to set a sampling data set based

on the sampling data  $S_{i,j}$ . That is, The receiving section 330 may set the sampling data set for selecting pixels, which the sampling data  $S_{i,j}$  used as the pixel data thereof, during the reception beam-forming

[0059] For example, the receiving section 330 may be configured to set the sampling data  $S_{1,1}, S_{1,4}, \dots, S_{1,r}, S_{2,1}, S_{2,4}, \dots, S_{2,r}, S_{p,r}$  as the sampling data set (denoted by a box) for selecting the pixels, which the sampling data  $S$  are used as the pixel data thereof, during the reception beam-forming, as shown in FIG. 14.

[0060] The receiving section 330 may be further configured to detect the pixels corresponding to the respective sampling data of the sampling data set based on the positions of the elements 311 and the positions (orientation) of the respective pixels of the ultrasound image UI with respect to the elements 311. That is, the receiving section 330 may select the pixels, which the respective sampling data of the sampling data set are used as the pixel data thereof, during the reception beam-forming based on the positions of the elements 311 and the orientation of the respective pixels of the ultrasound image UI with respect to the elements 311. The receiving section 330 may be further configured to cumulatively assign the sampling data to the selected pixels in the same manner as the above embodiments. The receiving section 330 may be also configured to perform the reception beam-forming upon the sampling data, which are cumulatively assigned to the respective pixels of the ultrasound image UI to form the reception-focused data.

[0061] In yet another embodiment, the receiving section 330 may be configured to perform down-sampling upon the reception signals provided through the plurality of channels  $CH_k$  from the ultrasound probe 310 to form down-sampled data. As described above, the receiving section 330 may be further configured to detect the pixels corresponding to the respective sampling data based on the positions of the elements 311 and the positions (orientation) of the respective pixels of the ultrasound image UI with respect to the elements 311. That is, the receiving section 330 may select the pixels, which the respective sampling data are used as the pixel data thereof, during the reception beam-forming based on the positions of the elements 311 and the orientation of the pixels of the ultrasound image UI with respect to the elements 311. The receiving section 330 may be further configured to cumulatively assign the respective sampling data to the selected pixels in the same manner as the above embodiments. The receiving section 330 may be further configured to perform the reception beam-forming upon the sampling data, which are cumulatively assigned to the respective pixels of the ultrasound image UI to form the reception-focused data.

[0062] However, it should be noted herein that the reception beam-forming may not be limited thereto.

[0063] Referring back to FIG. 3, the ultrasound data acquiring unit 120 may further include an ultrasound data forming section 340. The ultrasound data forming section 340 may be configured to form the ultrasound data corresponding to the ultrasound image based on the reception-focused data provided from the receiving section 330. The ultrasound data forming section 340 may be further configured to perform a signal process (e.g., gain control, etc) upon the reception-focused data.

[0064] In one embodiment, the ultrasound data forming section 340 may be configured to form ultrasound data (hereinafter referred to as "brightness mode ultrasound data") corresponding to the brightness mode image based on the bright-

ness mode reception-focused data provided from the receiving section 330. The brightness mode ultrasound data may include radio frequency data.

[0065] The ultrasound data forming section 340 may be further configured to form ultrasound data (hereinafter referred to as "Doppler mode ultrasound data") corresponding to the first region of interest ROI based on the Doppler mode reception-focused data provided from the receiving section 330. The Doppler mode ultrasound data may include in-phase/quadrature data. However, it should be noted herein that the Doppler mode ultrasound data may not be limited thereto.

[0066] For example, the ultrasound data forming section 340 may form first Doppler mode ultrasound data based on the first Doppler mode reception-focused data provided from the receiving section 330. The ultrasound data forming section 340 may further form second Doppler mode ultrasound data based on the second Doppler mode reception-focused data provided from the receiving section 330.

[0067] Referring back to FIG. 1, the ultrasound system 100 may further include a processing unit 130 in communication with the user input unit 110 and the ultrasound data acquiring unit 120. The processing unit 130 may include a central processing unit, a microprocessor, a graphic processing unit and the like.

[0068] FIG. 15 is a flow chart showing a process of forming motion profile information. The processing unit 130 may be configured to form the brightness mode image BI based on the brightness mode ultrasound data provided from the ultrasound data acquiring unit 120, at step S1502 in FIG. 15. The brightness mode image BI may be displayed on a display unit 150. Thus, the user may set the first region of interest ROI on the brightness mode image BI displayed on the display unit 150 by using the user input unit 110.

[0069] The processing unit 130 may be configured to set the first region of interest ROI on the brightness mode image BI based on the input information (i.e., first input information) provided from the user input unit 110, at step S1504 in FIG. 15. Thus, the ultrasound data acquiring unit 120 may be configured to transmit the ultrasound signals to the living body and receive the ultrasound echo signals from the living body to acquire the Doppler mode ultrasound data in consideration of the first region of interest ROI.

[0070] The processing unit 130 may be configured to form vector information based on the Doppler mode ultrasound data provided from the ultrasound data acquiring unit 120, at step S1506 in FIG. 15. That is, the processing unit 130 may form the vector information corresponding to motion (i.e., velocity and direction) of the target object based on the Doppler mode ultrasound data.

[0071] Generally, when the transmission direction of the ultrasound signals is equal to the reception direction of the ultrasound echo signals and a Doppler angle is  $\theta$ , the following relationship may be established:

$$X \cos \theta = \frac{C_0 f_d}{2 f_0} \quad (1)$$

[0072] In equation 1, X represents a reflector velocity (i.e., velocity of target object),  $C_0$  represents a sound speed in the living body,  $f_d$  represents a Doppler shift frequency, and  $f_0$  represents an ultrasound frequency.

[0073] The Doppler shift frequency  $f_d$  may be calculated by the difference between a frequency of the ultrasound signals (i.e., transmission beam) and a frequency of the ultrasound echo signals (i.e., reception beam). Also, the velocity component  $X \cos \theta$  projected to the transmission direction may be calculated by equation 1.

[0074] When the transmission direction of the ultrasound signals (i.e., transmission beam) is different to the reception direction of the ultrasound echo signals (i.e., reception beam), the following relationship may be established:

$$X \cos \theta_T + X \cos \theta_R = \frac{C_0 f_d}{f_0} \quad (2)$$

[0075] In equation 2,  $\theta_T$  represents an angle between the ultrasound signals (i.e., transmission beam) and the blood flow, and  $\theta_R$  represents an angle between the ultrasound echo signals (i.e., reception beam) and the blood flow.

[0076] FIG. 16 is a schematic diagram showing an example of the transmission directions, the reception directions, the vector information and an over-determined problem. Referring to FIG. 16, when the ultrasound signals (i.e., transmission beam) are transmitted in a first direction D1 and the ultrasound echo signals (i.e., reception beam) are received in the first direction D1, the following relationship may be established:

$$\vec{\alpha}_1 \vec{X} = \alpha_{11} x_1 + \alpha_{12} x_2 = y_1 = X \cos \theta \quad (3)$$

[0077] In equation 3,  $\vec{\alpha}_1 = (\alpha_{11}, \alpha_{12})$  represents a unit vector of the first direction D1,  $\vec{X} = (x_1, x_2)$  represents variables, and  $y_1$  is calculated by equation 1.

[0078] When the ultrasound signals (i.e., transmission beam) are transmitted in a second direction D2 and the ultrasound echo signals (i.e., reception beam) are received in a third direction D3, the following relationship may be established:

$$(\alpha_{21} + \alpha_{31}) x_1 + (\alpha_{22} + \alpha_{32}) x_2 = (y_2 + y_3) = X \cos \eta_2 + X \cos \eta_3 \quad (4)$$

[0079] Equations 3 and 4 assume a two-dimensional environment. However, equations 3 and 4 may be expanded to a three-dimensional environment. That is, when expanding equations 3 and 4 to the three-dimensional environment, the following relationship may be established:

$$\alpha_{11} x_1 + \alpha_{12} x_2 + \alpha_{13} x_3 = y \quad (5)$$

[0080] In the case of the two-dimensional environment (i.e., two-dimensional vector), at least two equations are required to calculate the variables  $x_1$  and  $x_2$ . For example, when the ultrasound signals (i.e., transmission beam) are transmitted in the third direction D3 and the ultrasound echo signals (i.e., reception beam) are received in the second direction D2 and a fourth direction D4 as shown in FIG. 16, the following equations may be established:

$$\begin{aligned} (\alpha_{31} + \alpha_{21}) x_1 + (\alpha_{32} + \alpha_{22}) x_2 &= (y_3 + y_2) \\ (\alpha_{31} + \alpha_{41}) x_1 + (\alpha_{32} + \alpha_{42}) x_2 &= (y_3 + y_4) \end{aligned} \quad (6)$$

[0081] The vector  $\vec{X} = (x_1, x_2)$  may be calculated by the equations of equation 6.

[0082] When the reception beam-forming is performed in at least two angles (i.e., at least two reception directions), at least two equations may be obtained and represented as the

over-determined problem, as shown in FIG. 16. The over-determined problem is well known in the art. Thus, it has not been described in detail so as not to unnecessarily obscure the present disclosure. The over-determined problem may be solved by a pseudo inverse method, a weighted least square method and the like based on noise characteristics added to the Doppler shift frequency. That is, MxN equations may be obtained by M transmission directions and the reception beam-forming of N reception directions at every transmission.

**[0083]** The processing unit 130 may be configured to form the Doppler mode image based on the vector information, at step S1508 in FIG. 15. The Doppler mode image may be displayed on the display unit 150. Thus, the user may set the at least one second region of interest on the Doppler mode image displayed on the display unit 150 by using the user input unit 110. For example, the user may set the second region of interest SP on the Doppler mode image VDI by moving a stroll bar SB, as shown in FIG. 17.

**[0084]** The processing unit 130 may be configured to set the second region of interest SP on the Doppler mode image VDI based on the input information (i.e., second input information) provided from the user input unit 110 as shown in FIG. 17, at step S1510 in FIG. 15.

**[0085]** The processing unit 130 may be configured to form the motion profile information corresponding to the second region of interest SP based on the vector information, at step S1512 in FIG. 15.

**[0086]** In one embodiment, the processing unit 130 may extract vector information corresponding to the second region of interest SP from the vector information. The processing unit 130 may further form the motion profile information corresponding to the second region of interest SP based on the extracted vector information. That is, the processing unit 130 may form the motion profile information for representing a velocity of the target object to a width of the target object based on the extracted vector information.

**[0087]** As one example, the processing unit 130 may form the motion profile information for representing the velocity of a first target object (e.g., blood flow) to the width of a second target object (e.g., blood vessel) based on the vector information corresponding to the second region of interest SP, as shown in FIG. 18.

**[0088]** As another example, the processing unit 130 may form the motion profile information for successively representing the velocity of the second target object (e.g., blood flow) to the width of the first target object (e.g., blood vessel) during a predetermined time based on the vector information corresponding to the second region of interest SP, as shown in FIG. 19. The second region of interest SP may be set at the same position or different position.

**[0089]** In another embodiment, the processing unit 130 may be configured to set the third region of interest DROI on the Doppler mode image VDI based on the input information (i.e., third input information for setting the third region of interest DROI on the Doppler mode image VDI) provided from the user input unit 110, as shown in FIG. 20. The processing unit 130 may be further configured to extract vector information (i.e., motion profile information) corresponding to the third region of interest DROI from the vector information. The processing unit 130 may be also configured to perform a three-dimensional rendering upon the extracted vector information to form three-dimensional profile information for representing the velocity of the second target

object (e.g., blood flow) to the width of the first target object (e.g., blood vessel), as shown in FIG. 22. The methods of performing the three-dimensional rendering are well known in the art. Thus, they have not been described in detail so as not to unnecessarily obscure the present disclosure.

**[0090]** In yet another embodiment, the processing unit 130 may be configured to set the third region of interest DROI on the motion profile information based on the input information (i.e., third input information for setting the third region of interest DROI on the motion profile information) provided from the user input unit 110, as shown in FIG. 21. The processing unit 130 may be further configured to extract vector information (i.e., motion profile information) corresponding to the third region of interest DROI from the vector information. The processing unit 130 may be also configured to perform the three-dimensional rendering upon the extracted vector information to form the three-dimensional motion profile information for representing the velocity of the second target object (e.g., blood flow) to the width of the first target object (e.g., blood vessel), as shown in FIG. 22.

**[0091]** In yet another embodiment, the processing unit 130 may be configured to set the third region of interest on the Doppler mode image VDI based on the input information (i.e., third input information for setting the third region of interest on the Doppler mode image VDI) provided from the user input unit 110. The processing unit 130 may be further configured to extract vector information corresponding to the third region of interest from the vector information. The processing unit 130 may be also configured to perform the three-dimensional rendering upon the extracted vector information to form the three-dimensional motion profile information for representing the velocity of the second target object (e.g., blood flow) to the width of the first target object (e.g., blood vessel). The third region of interest may be equal to or different from the first region of interest ROI.

**[0092]** In yet another embodiment, the processing unit 130 may be configured to set the third region of interest on the Doppler mode image VDI based on the input information (i.e., third input information for setting the third region of interest on the Doppler mode image VDI) provided from the user input unit 110. The processing unit 130 may be further configured to extract vector information corresponding to the third region of interest from the vector information. The processing unit 130 may be additionally configured to perform the three-dimensional rendering upon the extracted vector information to form the three-dimensional motion profile information for representing the velocity of the second target object (e.g., blood flow) to the width of the first target object (e.g., blood vessel). The processing unit 130 may be also configured to map the three-dimensional motion profile information to the Doppler mode image (i.e., brightness mode image BI), as shown in FIG. 23.

**[0093]** Referring back to FIG. 1, the ultrasound system 100 may further include the storage unit 140. The storage unit 140 may store the ultrasound data (i.e., brightness mode ultrasound data and Doppler mode ultrasound data) acquired by the ultrasound data acquiring unit 120. The storage unit 140 may additionally store the vector information formed by the processing unit 130.

**[0094]** The ultrasound system 100 may further include the display unit 150. The display unit 150 may be configured to display the brightness mode image BI formed by the processing unit 130. The display unit 150 may be further configured to display the Doppler mode image VDI formed by the pro-

cessing unit **130**. The display unit **150** may be also configured to display the motion profile information formed by the processing unit **130**.

**[0095]** Although embodiments have been described with reference to a number of illustrative embodiments thereof, it should be understood that numerous other modifications and embodiments can be devised by those skilled in the art that will fall within the spirit and scope of the principles of this disclosure. More particularly, numerous variations and modifications are possible in the component parts and/or arrangements of the subject combination arrangement within the scope of the disclosure, the drawings and the appended claims. In addition to variations and modifications in the component parts and/or arrangements, alternative uses will also be apparent to those skilled in the art.

What is claimed is:

1. An ultrasound system, comprising:
  - a processing unit configured to form vector information of a target object based on ultrasound data corresponding to the target object, form a Doppler mode image based on the vector information, and set a first region of interest on the Doppler mode image based on input information of a user, the processing unit being further configured to form motion profile information corresponding to a motion of the target object based on vector information corresponding to the first region of interest.
  2. The ultrasound system of claim **1**, wherein the processing unit is configured to form the vector information corresponding to a velocity and a direction of the target object in consideration of at least one transmission direction and at least one reception direction corresponding to the at least one transmission direction based on the ultrasound data.
  3. The ultrasound system of claim **1**, further comprising:
    - a user input unit configured to receive the input information for setting the first region of interest on the Doppler mode image from the user.
  4. The ultrasound system of claim **3**, wherein the processing unit is configured to:
    - extract vector information corresponding to the first region of interest from the vector information; and
    - form the motion profile information based on the vector information corresponding to the first region of interest.
  5. The ultrasound system of claim **4**, wherein the processing unit is configured to form the motion profile information for representing a velocity of the target object to a width of the target object based on the vector information corresponding to the first region of interest.
  6. The ultrasound system of claim **4**, wherein the processing unit is configured to form the motion profile information for successively representing a velocity of the target object to a width of the target object during a predetermined time based on the vector information corresponding to the first region of interest.
  7. The ultrasound system of claim **4**, wherein the processing unit is configured to perform a three-dimensional rendering upon the vector information corresponding to the first region of interest to form the motion profile information for representing a velocity of the target object to a width of the target object.
  8. The ultrasound system of claim **4**, wherein the processing unit is configured to:
    - perform a three-dimensional rendering upon the vector information corresponding to the first region of interest

to form the motion profile information for representing a velocity of the target object to a width of the target object; and

map the motion profile information to the Doppler mode image.

9. The ultrasound system of claim **1**, further comprising:
  - a user input unit configured to receive the input information for setting a second region of interest on the Doppler mode image or the motion profile information from the user.
10. The ultrasound system of claim **9**, wherein the processing unit is configured to:
  - set the second region of interest on the Doppler mode image;
  - extract vector information corresponding to the second region of interest from the vector information; and
  - perform a three-dimensional rendering upon the vector information corresponding to the second region of interest to form three-dimensional motion profile information.
11. The ultrasound system of claim **9**, wherein the processing unit is configured to:
  - set the second region of interest on the motion profile information;
  - extract vector information corresponding to the second region of interest from the vector information; and
  - perform a three-dimensional rendering upon the vector information corresponding to the second region of interest to form three-dimensional motion profile information.
12. The ultrasound system of claim **1**, further comprising:
  - an ultrasound data acquiring unit configured to transmit ultrasound signals to a living body including the target object in at least one transmission direction, and receive ultrasound echo signals from the living body in at least one reception direction to acquire the ultrasound data corresponding to the at least one reception direction.
13. The ultrasound system of claim **12**, wherein the ultrasound data acquiring unit is configured to:
  - transmit the ultrasound signals to the living body in a first transmission direction; and
  - receive the ultrasound echo signals from the living body in a first reception direction and a second reception direction to acquire the ultrasound data corresponding to the respective first and second reception directions.
14. The ultrasound system of claim **12**, wherein the ultrasound data acquiring unit is configured to:
  - transmit the ultrasound signals to the living body in a first transmission direction and a second transmission direction; and
  - receive the ultrasound echo signals from the living body in a first reception direction to acquire the ultrasound data corresponding to the first reception direction of the respective first and second transmission directions.
15. The ultrasound system of claim **12**, wherein the ultrasound data acquiring unit is configured to:
  - transmit the ultrasound signals to the living body in a first transmission direction and a second transmission direction; and
  - receive the ultrasound echo signals from the living body in a first reception direction and a second reception direction to acquire the ultrasound data corresponding to the respective first and second reception directions.

**16.** The ultrasound system of claim **12**, wherein the ultrasound data acquiring unit is configured to transmit the ultrasound signals in an interleaved transmission scheme.

**17.** The ultrasound system of claim **12**, wherein the ultrasound signals include plane wave signals or focused signals.

**18.** A method of providing motion profile information, comprising:

- a) forming vector information of a target object based on ultrasound data corresponding to the target object;
- b) forming a Doppler mode image based on the vector information;
- c) setting a first region of interest on the Doppler mode image based on input information of a user; and
- d) forming motion profile information corresponding to a motion of the target object based on the vector information corresponding to the first region of interest.

**19.** The method of claim **18**, wherein the step a) comprises: forming the vector information corresponding to a velocity and a direction of the target object in consideration of at least one transmission direction and at least one reception direction corresponding to the at least one transmission direction based on the ultrasound data.

**20.** The method of claim **18**, further comprising: receiving the input information for setting the first region of interest on the Doppler mode image from the user, prior to performing the step c).

**21.** The method of claim **20**, wherein the step d) comprises: extracting vector information corresponding to the first region of interest from the vector information; and forming the motion profile information based on the vector information corresponding to the first region of interest.

**22.** The method of claim **21**, wherein the step d) comprises: forming the motion profile information for representing a velocity of the target object to a width of the target object based on the vector information corresponding to the first region of interest.

**23.** The method of claim **21**, wherein the step d) comprises: forming the motion profile information for successively representing a velocity of the target object to a width of the target object during a predetermined time based on the vector information corresponding to the first region of interest.

**24.** The method of claim **21**, wherein the step d) comprises: performing a three-dimensional rendering upon the vector information corresponding to the first region of interest to form the motion profile information for representing a velocity of the target object to a width of the target object.

**25.** The method of claim **21**, wherein the step d) comprises: performing a three-dimensional rendering upon the vector information corresponding to the first region of interest to form the motion profile information for representing a velocity of the target object to a width of the target object; and mapping the motion profile information to the Doppler mode image.

**26.** The method of claim **18**, further comprising:

e) receiving input information for setting a second region of interest on the Doppler mode image or the motion profile information from the user.

**27.** The method of claim **26**, further comprising:

- f) setting the second region of interest on the Doppler mode image based on the input information;
- g) extracting vector information corresponding to the second region of interest from the vector information; and
- h) performing a three-dimensional rendering upon the vector information corresponding to the second region of interest to form three-dimensional profile information.

**28.** The method of claim **26**, further comprising:

- f) setting the second region of interest on the motion profile information based on the input information;
- g) extracting vector information corresponding to the second region of interest from the vector information; and
- h) performing a three-dimensional rendering upon the vector information corresponding to the second region of interest to form three-dimensional motion profile information.

**29.** The method of claim **18**, further comprising:

transmitting ultrasound signals to a living body including the target object in at least one transmission direction and receiving ultrasound echo signals from the living body in at least one reception direction to acquire the ultrasound data corresponding to the at least one reception direction, prior to performing the step a).

**30.** The method of claim **29**, wherein the step of acquiring the ultrasound data comprises:

transmitting the ultrasound signals to the living body in a first transmission direction; and receiving the ultrasound echo signals from the living body in a first reception direction and a second reception direction to acquire the ultrasound data corresponding to the respective first and second reception directions.

**31.** The method of claim **29**, wherein the step of acquiring the ultrasound data comprises:

transmitting the ultrasound signals to the living body in a first transmission direction and a second transmission direction; and receiving the ultrasound echo signals from the living body in a first reception direction to acquire the ultrasound data corresponding to the first reception direction of the respective first and second transmission directions.

**32.** The method of claim **29**, wherein the step of acquiring the ultrasound data comprises:

transmitting the ultrasound signals to the living body in a first transmission direction and a second transmission direction; and receiving the ultrasound echo signals from the living body in a first reception direction and a second reception direction to acquire the ultrasound data corresponding to the respective first and second reception directions.

**33.** The method of claim **29**, wherein the ultrasound signals are transmitted in an interleaved transmission scheme.

**34.** The method of claim **29**, wherein the ultrasound signals include plane wave signals or focused signals.

\* \* \* \* \*

FIG. 4

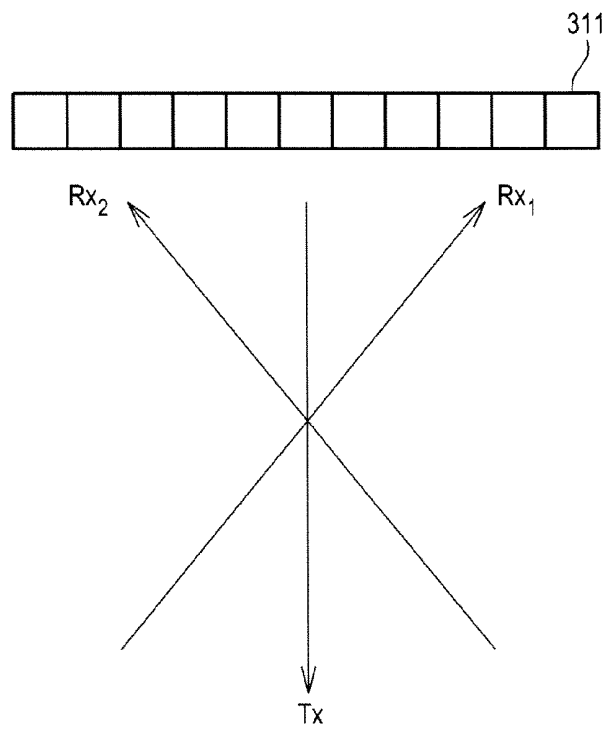


FIG. 5

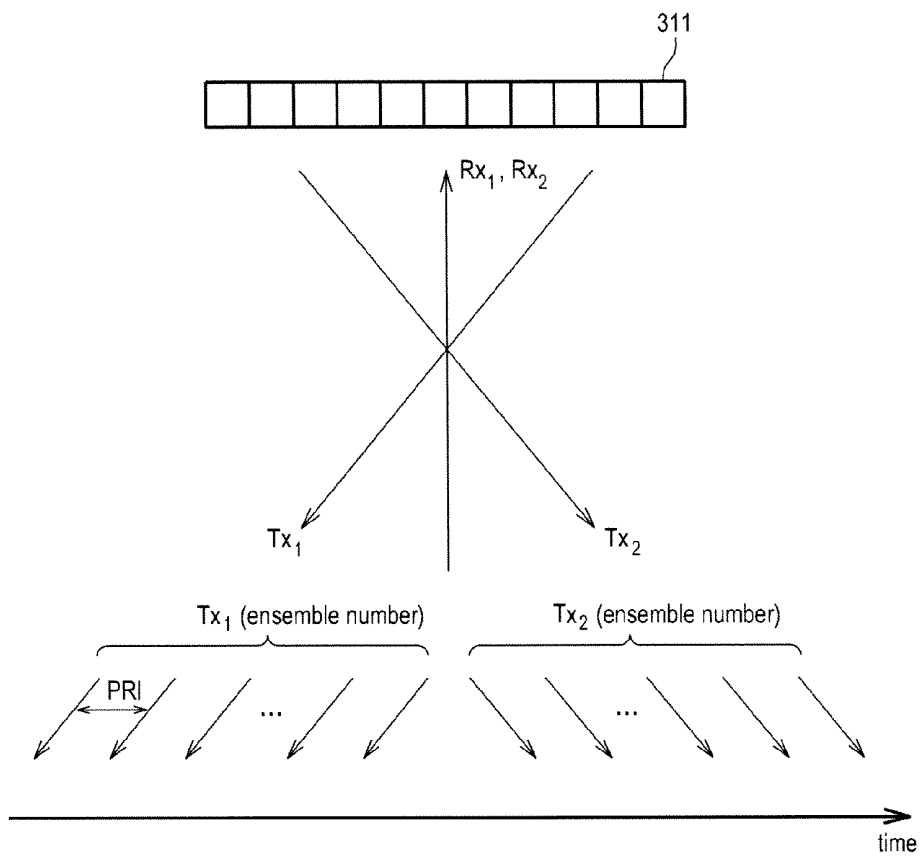


FIG. 6

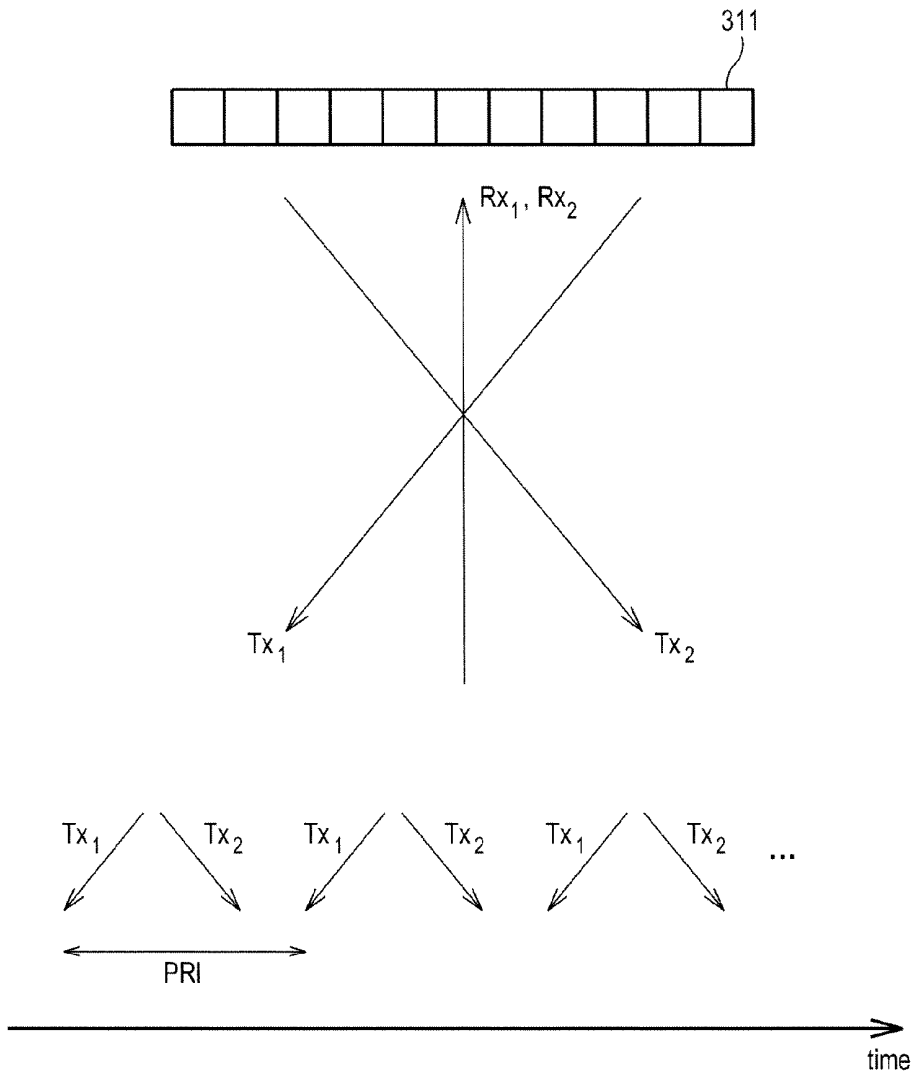


FIG. 7

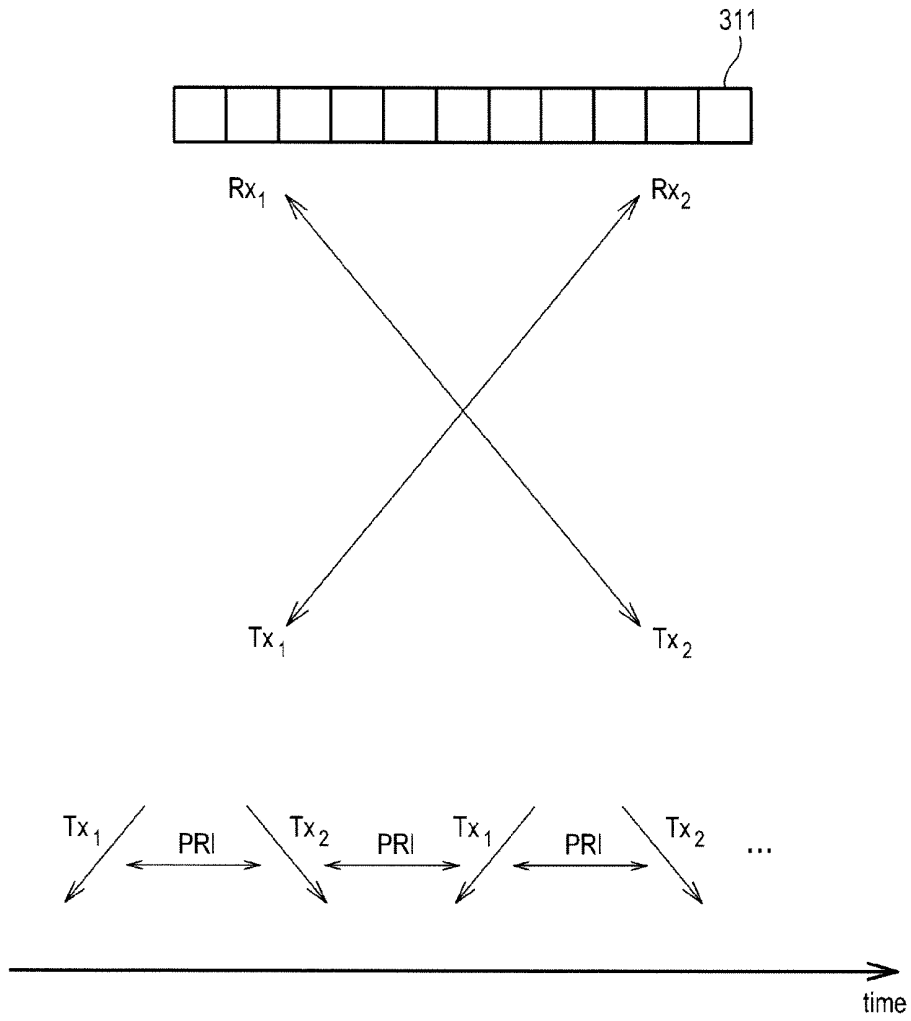


FIG. 8

$S_{1,t}$	$S_{2,t}$	$S_{3,t}$	$S_{4,t}$	$S_{5,t}$	$S_{6,t}$	$S_{7,t}$	$S_{8,t}$	$S_{9,t}$	$S_{10,t}$	$S_{11,t}$	...	$S_{p,t}$
$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$
$S_{1,6}$	$S_{2,6}$	$S_{3,6}$	$S_{4,6}$	$S_{5,6}$	$S_{6,6}$	$S_{7,6}$	$S_{8,6}$	$S_{9,6}$	$S_{10,6}$	$S_{11,6}$	...	$S_{p,6}$
$S_{1,5}$	$S_{2,5}$	$S_{3,5}$	$S_{4,5}$	$S_{5,5}$	$S_{6,5}$	$S_{7,5}$	$S_{8,5}$	$S_{9,5}$	$S_{10,5}$	$S_{11,5}$	...	$S_{p,5}$
$S_{1,4}$	$S_{2,4}$	$S_{3,4}$	$S_{4,4}$	$S_{5,4}$	$S_{6,4}$	$S_{7,4}$	$S_{8,4}$	$S_{9,4}$	$S_{10,4}$	$S_{11,4}$	...	$S_{p,4}$
$S_{1,3}$	$S_{2,3}$	$S_{3,3}$	$S_{4,3}$	$S_{5,3}$	$S_{6,3}$	$S_{7,3}$	$S_{8,3}$	$S_{9,3}$	$S_{10,3}$	$S_{11,3}$	...	$S_{p,3}$
$S_{1,2}$	$S_{2,2}$	$S_{3,2}$	$S_{4,2}$	$S_{5,2}$	$S_{6,2}$	$S_{7,2}$	$S_{8,2}$	$S_{9,2}$	$S_{10,2}$	$S_{11,2}$	...	$S_{p,2}$
$S_{1,1}$	$S_{2,1}$	$S_{3,1}$	$S_{4,1}$	$S_{5,1}$	$S_{6,1}$	$S_{7,1}$	$S_{8,1}$	$S_{9,1}$	$S_{10,1}$	$S_{11,1}$	...	$S_{p,1}$

CH <sub>1</sub>	CH <sub>2</sub>	CH <sub>3</sub>	CH <sub>4</sub>	CH <sub>5</sub>	CH <sub>6</sub>	CH <sub>7</sub>	CH <sub>8</sub>	CH <sub>9</sub>	CH <sub>10</sub>	CH <sub>11</sub>	...	CH <sub>p</sub>
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P <sub>1,1</sub>	P <sub>1,2</sub>	P <sub>1,3</sub>	P <sub>1,4</sub>	P <sub>1,5</sub>	P <sub>1,6</sub>	P <sub>1,7</sub>	P <sub>1,8</sub>	P <sub>1,9</sub>	...	P <sub>1,N</sub>
P <sub>2,1</sub>	P <sub>2,2</sub>	P <sub>2,3</sub>	P <sub>2,4</sub>	P <sub>2,5</sub>	P <sub>2,6</sub>	P <sub>2,7</sub>	P <sub>2,8</sub>	P <sub>2,9</sub>	...	P <sub>2,N</sub>
P <sub>3,1</sub>	P <sub>3,2</sub>	P <sub>3,3</sub>	P <sub>3,4</sub>	P <sub>3,5</sub>	P <sub>3,6</sub>	P <sub>3,7</sub>	P <sub>3,8</sub>	P <sub>3,9</sub>	...	P <sub>3,N</sub>
P <sub>4,1</sub>	P <sub>4,2</sub>	P <sub>4,3</sub>	P <sub>4,4</sub>	P <sub>4,5</sub>	P <sub>4,6</sub>	P <sub>4,7</sub>	P <sub>4,8</sub>	P <sub>4,9</sub>	...	P <sub>4,N</sub>
P <sub>5,1</sub>	P <sub>5,2</sub>	P <sub>5,3</sub>	P <sub>5,4</sub>	P <sub>5,5</sub>	P <sub>5,6</sub>	P <sub>5,7</sub>	P <sub>5,8</sub>	P <sub>5,9</sub>	...	P <sub>5,N</sub>
P <sub>6,1</sub>	P <sub>6,2</sub>	P <sub>6,3</sub>	P <sub>6,4</sub>	P <sub>6,5</sub>	P <sub>6,6</sub>	P <sub>6,7</sub>	P <sub>6,8</sub>	P <sub>6,9</sub>	...	P <sub>6,N</sub>
P <sub>7,1</sub>	P <sub>7,2</sub>	P <sub>7,3</sub>	P <sub>7,4</sub>	P <sub>7,5</sub>	P <sub>7,6</sub>	P <sub>7,7</sub>	P <sub>7,8</sub>	P <sub>7,9</sub>	...	P <sub>7,N</sub>
$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$
P <sub>M,1</sub>	P <sub>M,2</sub>	P <sub>M,3</sub>	P <sub>M,4</sub>	P <sub>M,5</sub>	P <sub>M,6</sub>	P <sub>M,7</sub>	P <sub>M,8</sub>	P <sub>M,9</sub>	...	P <sub>M,N</sub>

UI

FIG. 9

$S_{1,t}$	$S_{2,t}$	$S_{3,t}$	$S_{4,t}$	$S_{5,t}$	$S_{6,t}$	$S_{7,t}$	$S_{8,t}$	$S_{9,t}$	$S_{10,t}$	$S_{11,t}$	...	$S_{p,t}$
$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$
$S_{1,6}$	$S_{2,6}$	$S_{3,6}$	$S_{4,6}$	$S_{5,6}$	$S_{6,6}$	$S_{7,6}$	$S_{8,6}$	$S_{9,6}$	$S_{10,6}$	$S_{11,6}$	...	$S_{p,6}$
$S_{1,5}$	$S_{2,5}$	$S_{3,5}$	$S_{4,5}$	$S_{5,5}$	$S_{6,5}$	$S_{7,5}$	$S_{8,5}$	$S_{9,5}$	$S_{10,5}$	$S_{11,5}$	...	$S_{p,5}$
$S_{1,4}$	$S_{2,4}$	$S_{3,4}$	$S_{4,4}$	$S_{5,4}$	$S_{6,4}$	$S_{7,4}$	$S_{8,4}$	$S_{9,4}$	$S_{10,4}$	$S_{11,4}$	...	$S_{p,4}$
$S_{1,3}$	$S_{2,3}$	$S_{3,3}$	$S_{4,3}$	$S_{5,3}$	$S_{6,3}$	$S_{7,3}$	$S_{8,3}$	$S_{9,3}$	$S_{10,3}$	$S_{11,3}$	...	$S_{p,3}$
$S_{1,2}$	$S_{2,2}$	$S_{3,2}$	$S_{4,2}$	$S_{5,2}$	$S_{6,2}$	$S_{7,2}$	$S_{8,2}$	$S_{9,2}$	$S_{10,2}$	$S_{11,2}$	...	$S_{p,2}$
$S_{1,1}$	$S_{2,1}$	$S_{3,1}$	$S_{4,1}$	$S_{5,1}$	$S_{6,1}$	$S_{7,1}$	$S_{8,1}$	$S_{9,1}$	$S_{10,1}$	$S_{11,1}$	...	$S_{p,1}$
$CH_1$	$CH_2$	$CH_3$	$CH_4$	$CH_5$	$CH_6$	$CH_7$	$CH_8$	$CH_9$	$CH_{10}$	$CH_{11}$	...	$CH_p$

$P_{1,1}$	$P_{1,2}$	$P_{1,3}$	$P_{1,4}$	$P_{1,5}$	$P_{1,6}$	$P_{1,7}$	$P_{1,8}$	$P_{1,9}$	...	$P_{1,N}$
$P_{2,1}$	$P_{2,2}$	$P_{2,3}$	$P_{2,4}$	$P_{2,5}$	$P_{2,6}$	$P_{2,7}$	$P_{2,8}$	$P_{2,9}$	...	$P_{2,N}$
$P_{3,1}$	$P_{3,2}$	$P_{3,3}$	$P_{3,4}$	$P_{3,5}$	$P_{3,6}$	$P_{3,7}$	$P_{3,8}$	$P_{3,9}$	...	$P_{3,N}$
$P_{4,1}$	$P_{4,2}$	$P_{4,3}$	$P_{4,4}$	$P_{4,5}$	$P_{4,6}$	$P_{4,7}$	$P_{4,8}$	$P_{4,9}$	...	$P_{4,N}$
$P_{5,1}$	$P_{5,2}$	$P_{5,3}$	$P_{5,4}$	$P_{5,5}$	$P_{5,6}$	$P_{5,7}$	$P_{5,8}$	$P_{5,9}$	...	$P_{5,N}$
$P_{6,1}$	$P_{6,2}$	$P_{6,3}$	$P_{6,4}$	$P_{6,5}$	$P_{6,6}$	$P_{6,7}$	$P_{6,8}$	$P_{6,9}$	...	$P_{6,N}$
$P_{7,1}$	$P_{7,2}$	$P_{7,3}$	$P_{7,4}$	$P_{7,5}$	$P_{7,6}$	$P_{7,7}$	$P_{7,8}$	$P_{7,9}$	...	$P_{7,N}$
$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$
$P_{M,1}$	$P_{M,2}$	$P_{M,3}$	$P_{M,4}$	$P_{M,5}$	$P_{M,6}$	$P_{M,7}$	$P_{M,8}$	$P_{M,9}$	...	$P_{M,N}$

$CV_{6,3}$   
 UI



专利名称(译)	提供超声系统中目标物体的运动轮廓信息		
公开(公告)号	<a href="#">US20130165784A1</a>	公开(公告)日	2013-06-27
申请号	US13/728609	申请日	2012-12-27
[标]申请(专利权)人(译)	三星麦迪森株式会社		
当前申请(专利权)人(译)	三星MEDISON CO. , LTD.		
[标]发明人	KIM NAM WOONG CHOI SEOK WON LEE HAN WOO		
发明人	KIM, NAM WOONG CHOI, SEOK WON LEE, HAN WOO		
IPC分类号	A61B8/08 A61B8/06 A61B8/02 A61B8/14 A61B8/00		
CPC分类号	A61B8/5246 A61B8/488 A61B8/145 A61B8/463 A61B8/5207 A61B8/4488 A61B8/483 A61B8/466 A61B8/02 A61B8/06 A61B8/4444 A61B8/469		
优先权	1020110143827 2011-12-27 KR		
外部链接	<a href="#">Espacenet</a> <a href="#">USPTO</a>		

摘要(译)

提供了用于通过使用矢量多普勒来提供与目标对象的运动相对应的运动轮廓信息的实施例。在一个实施例中，作为非限制性示例，超声系统包括：处理单元，被配置为基于与目标对象相对应的超声数据形成目标对象的矢量信息，基于矢量信息形成多普勒模式图像，基于用户的输入信息在多普勒模式图像上设置第一感兴趣区域，处理单元还被配置为基于与第一感兴趣区域对应的矢量信息形成与目标对象的运动对应的运动轮廓信息。。

