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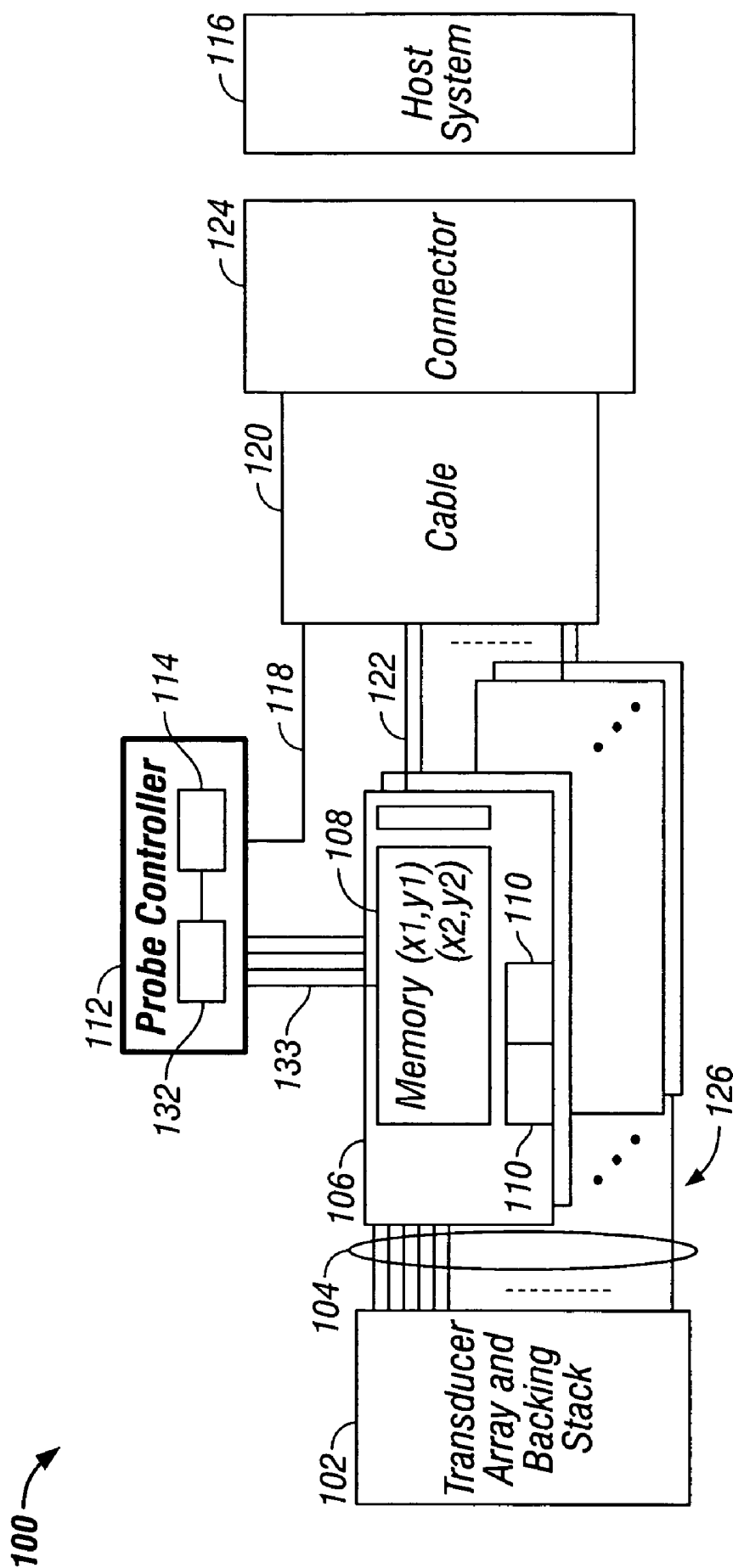


FIG. 1

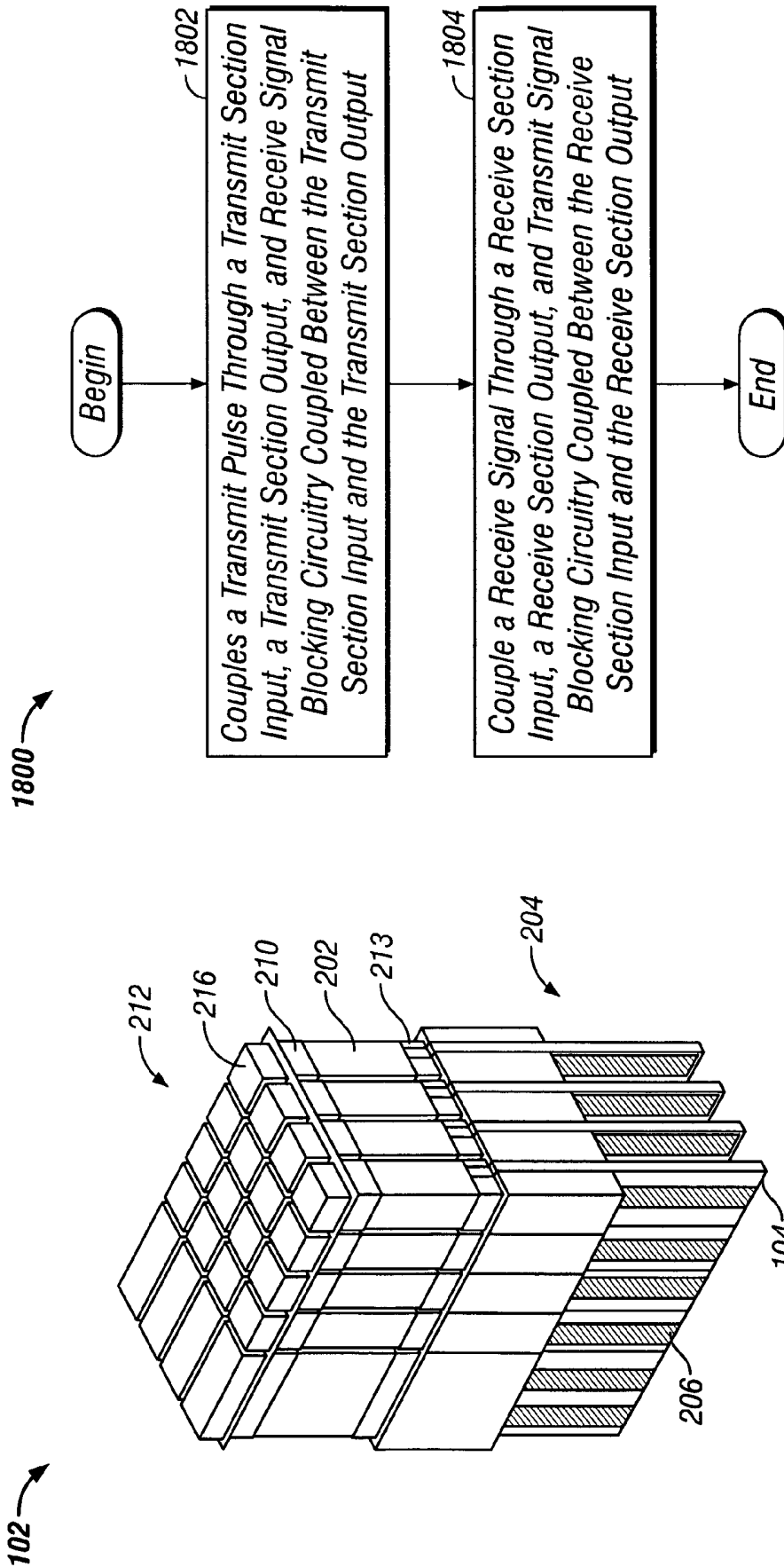


FIG. 2

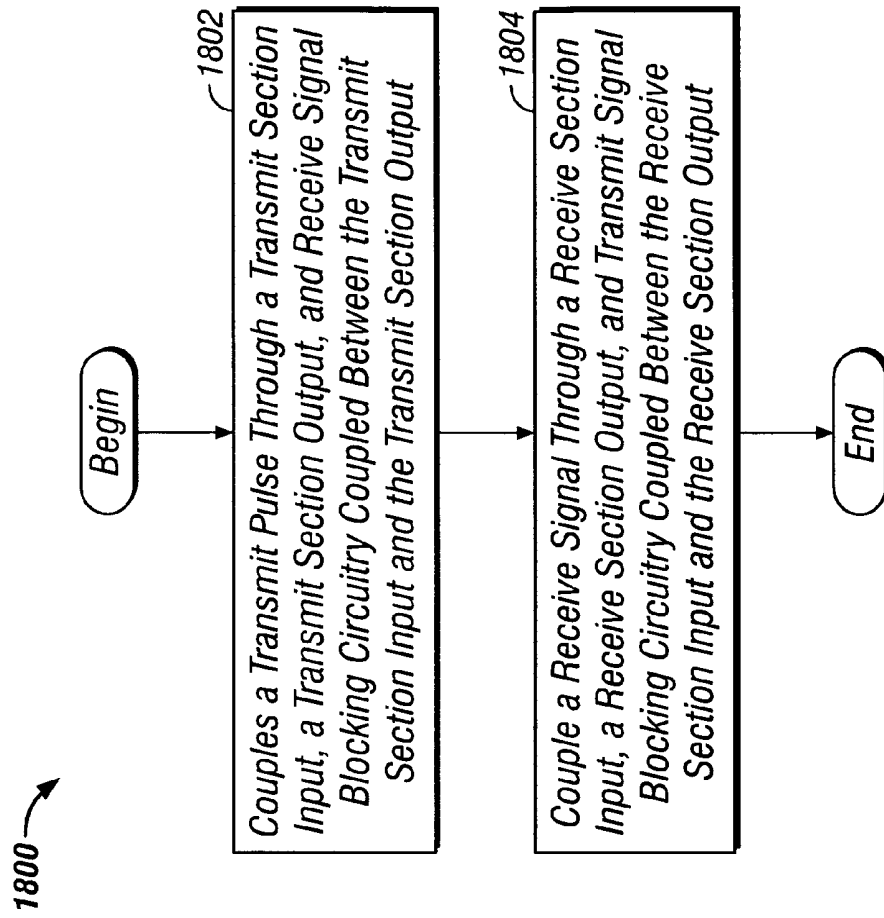


FIG. 18

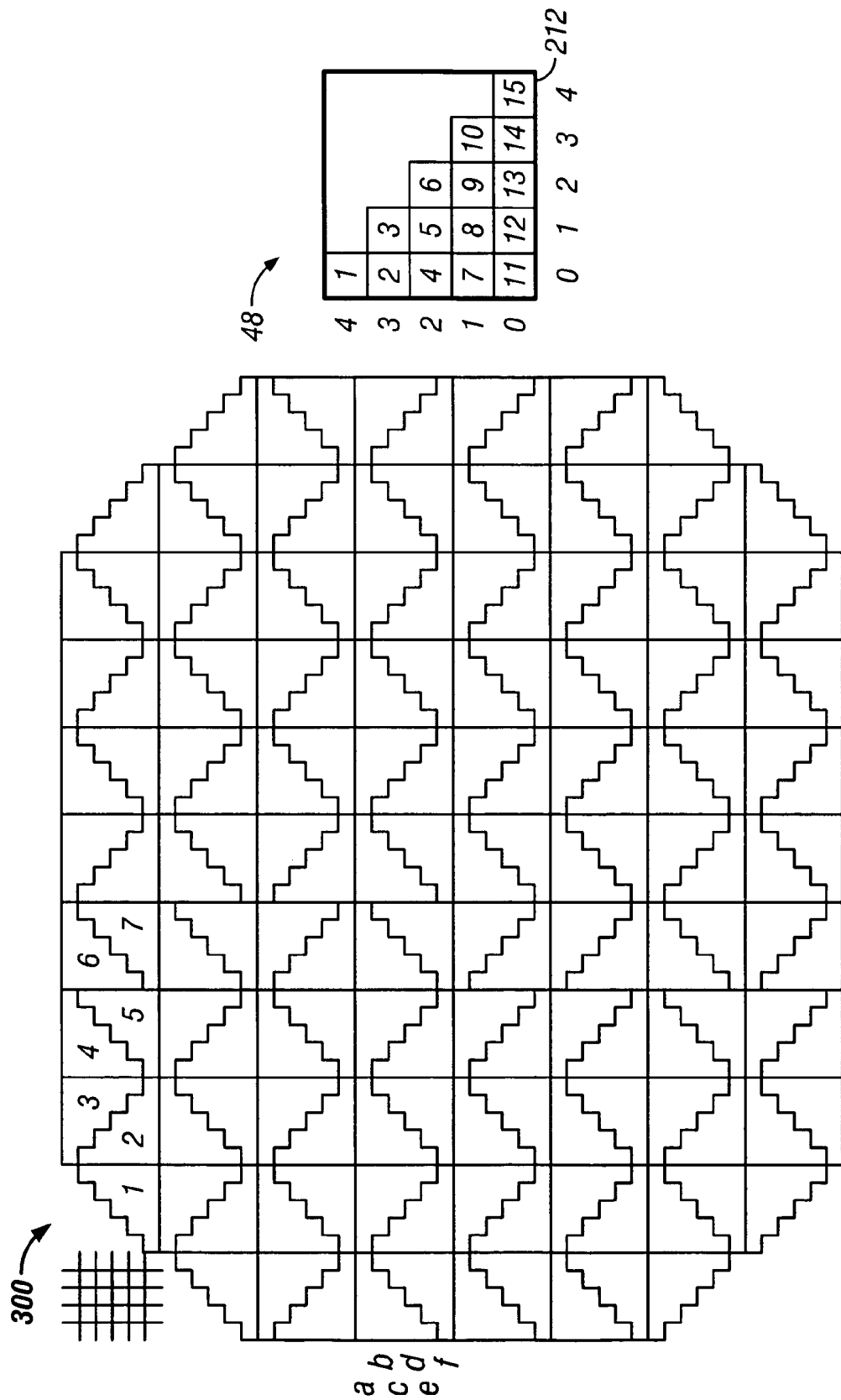


FIG. 3

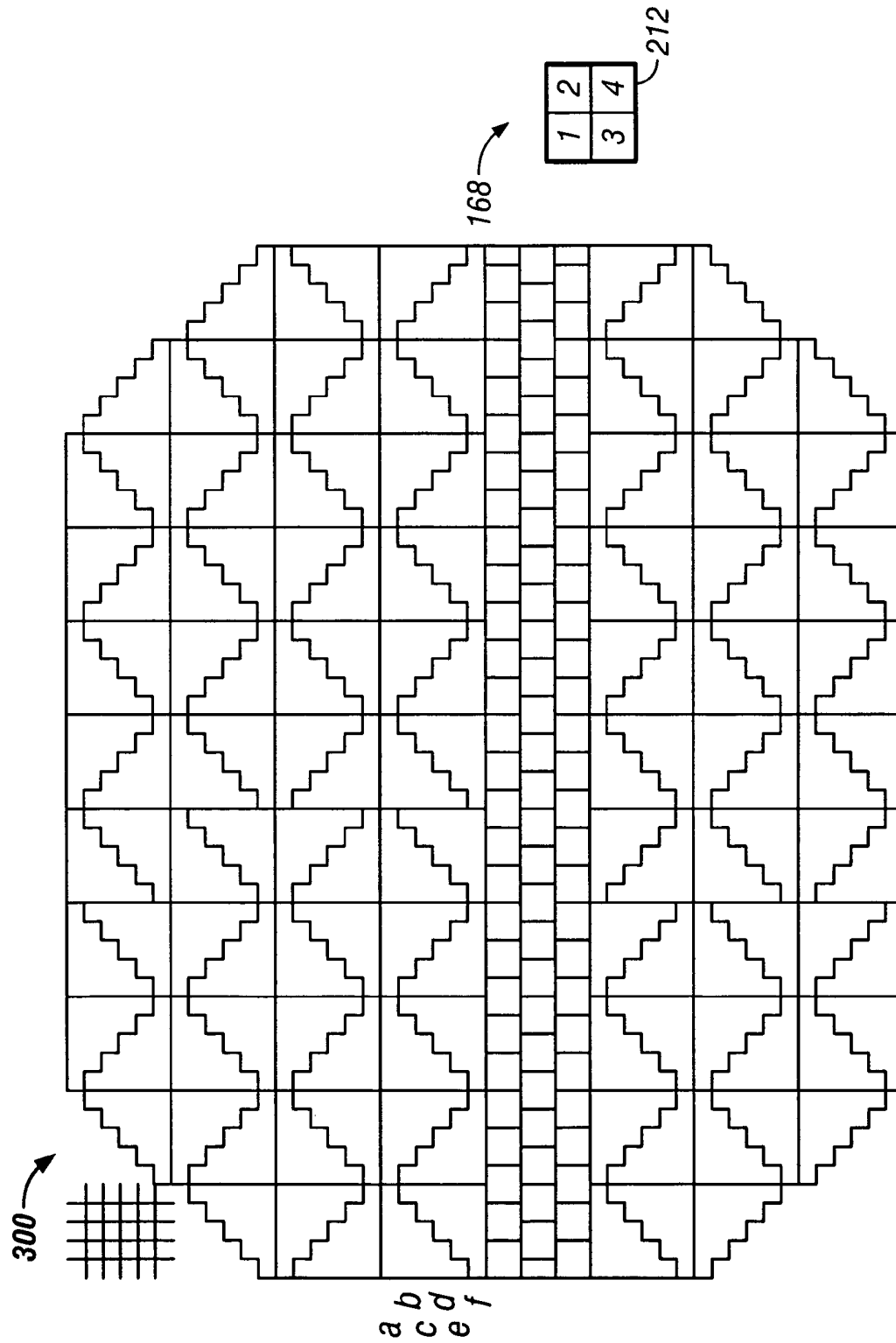


FIG. 4

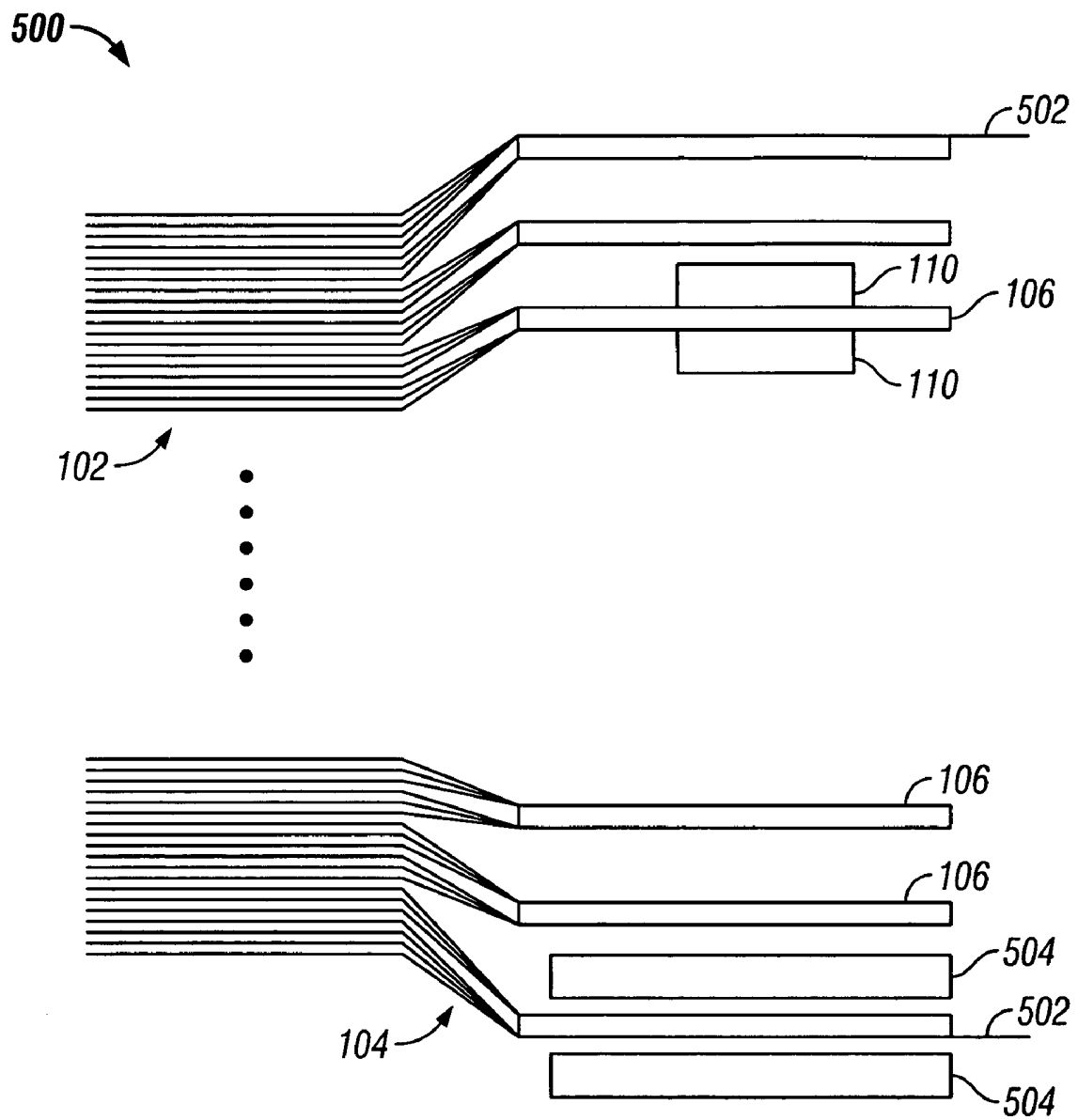
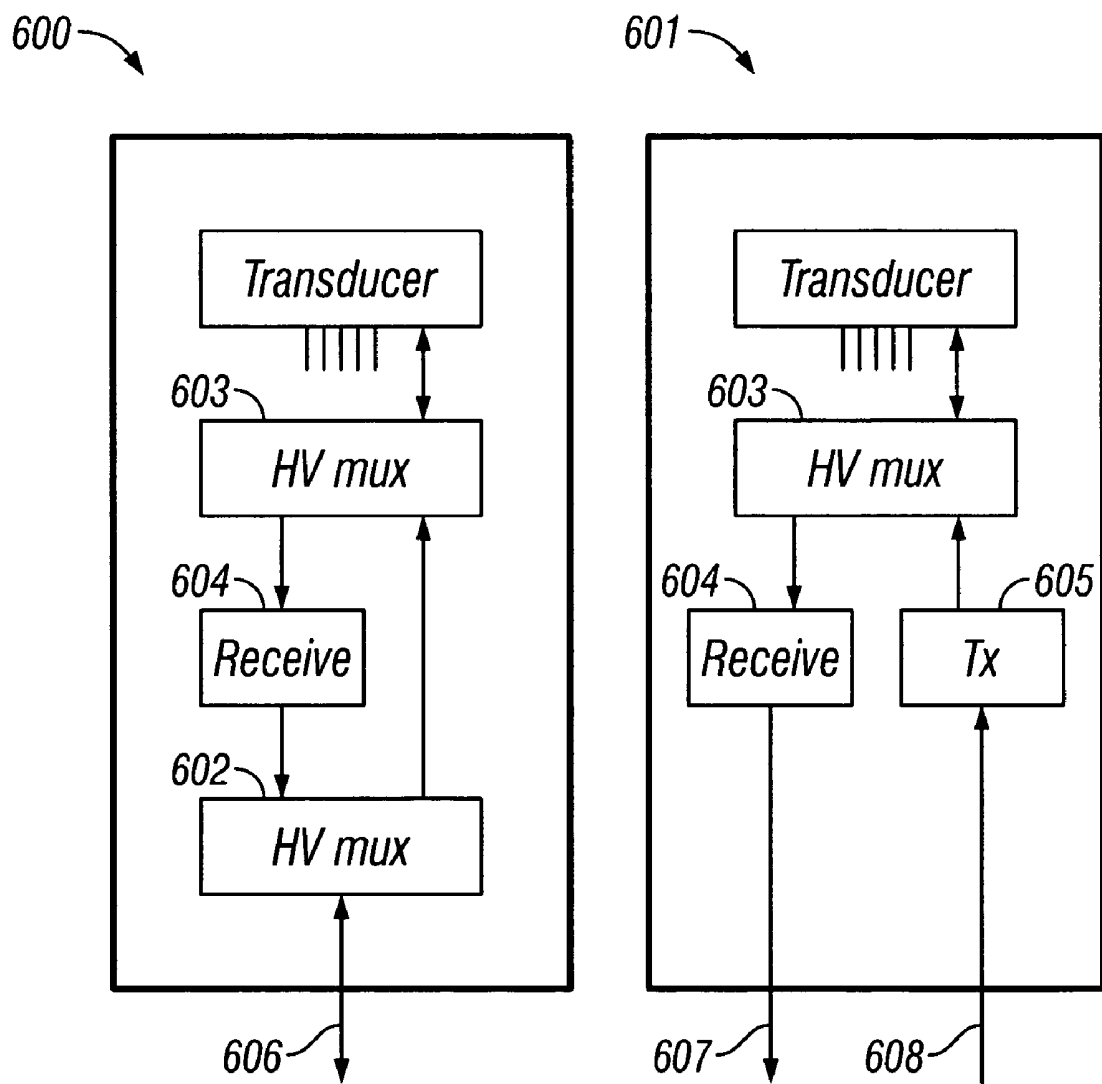


FIG. 5

**FIG. 6**

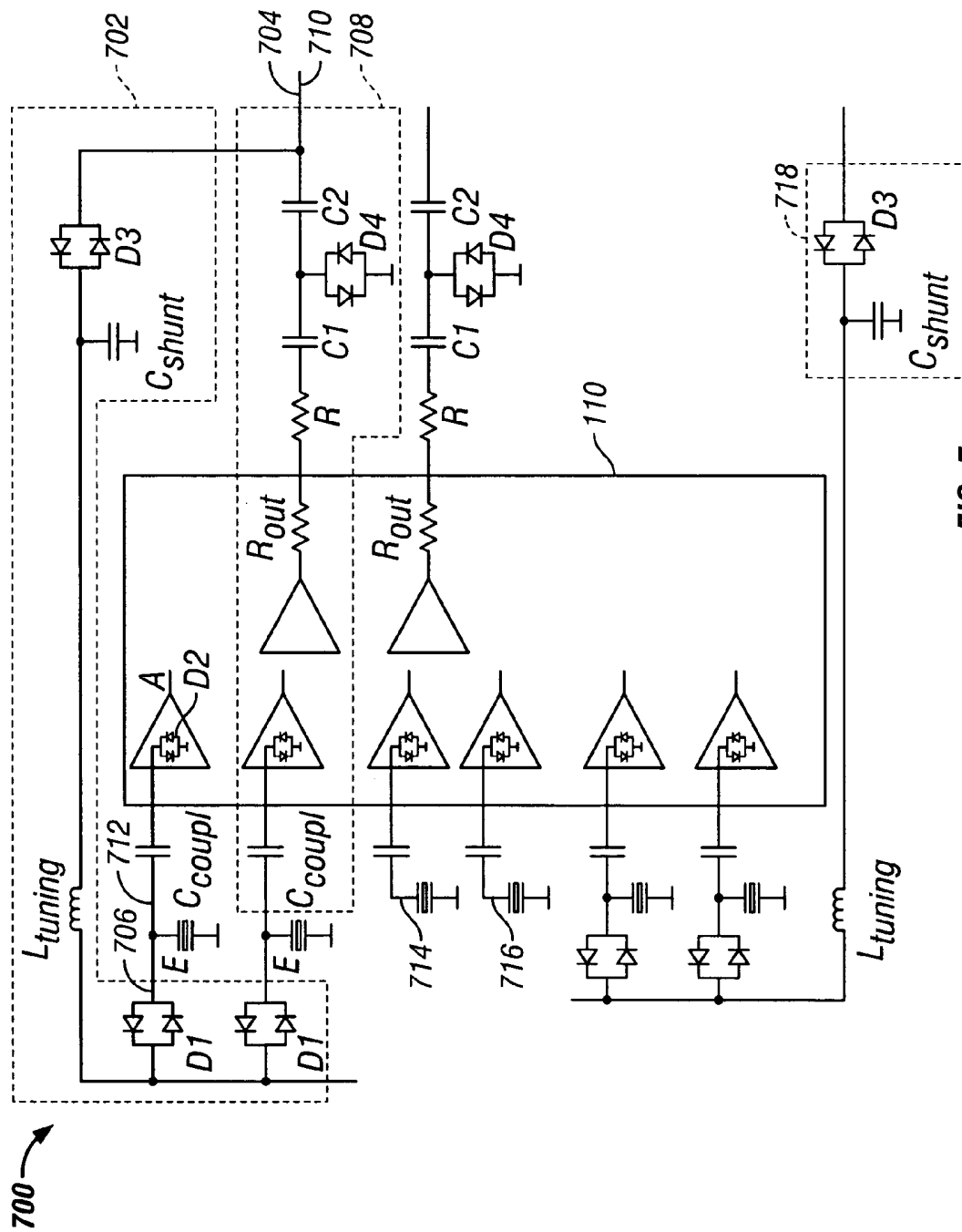
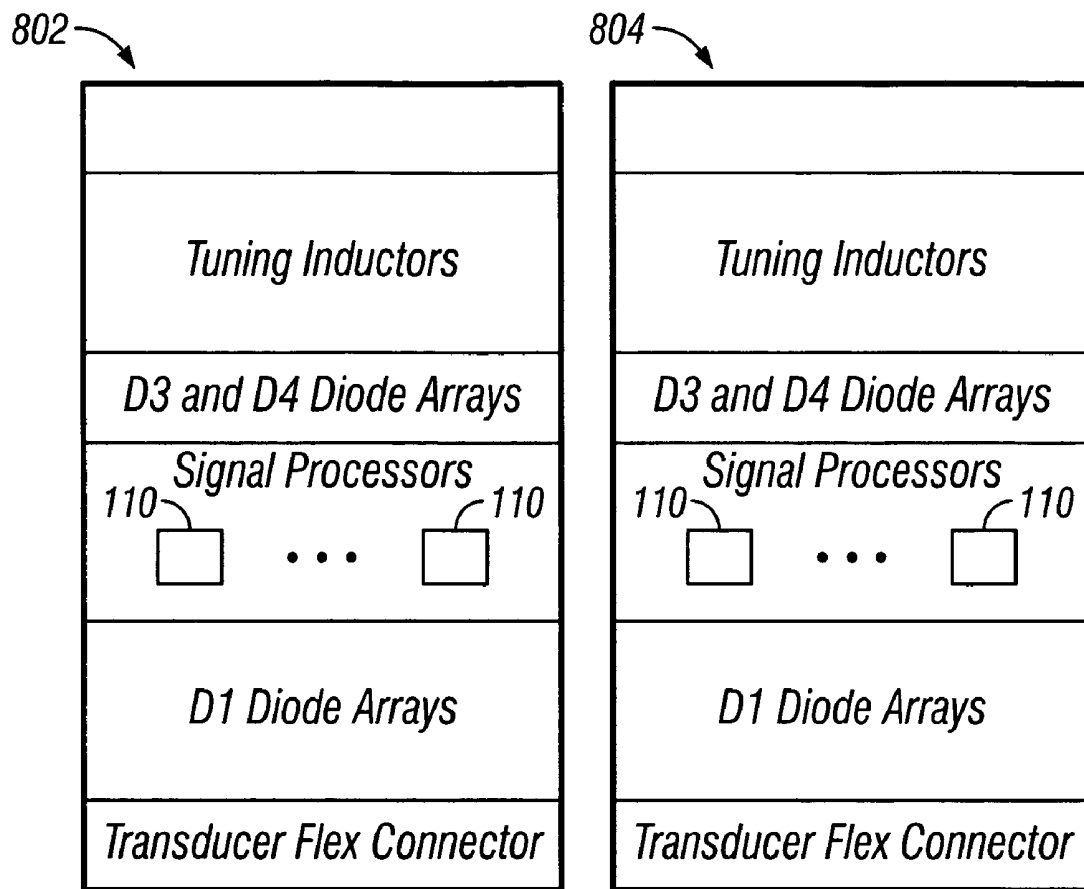
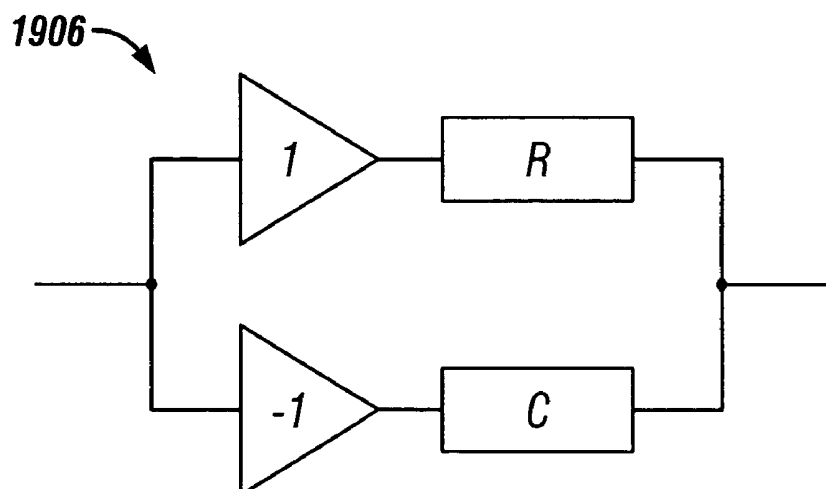


FIG. 7

**FIG. 8****FIG. 11**

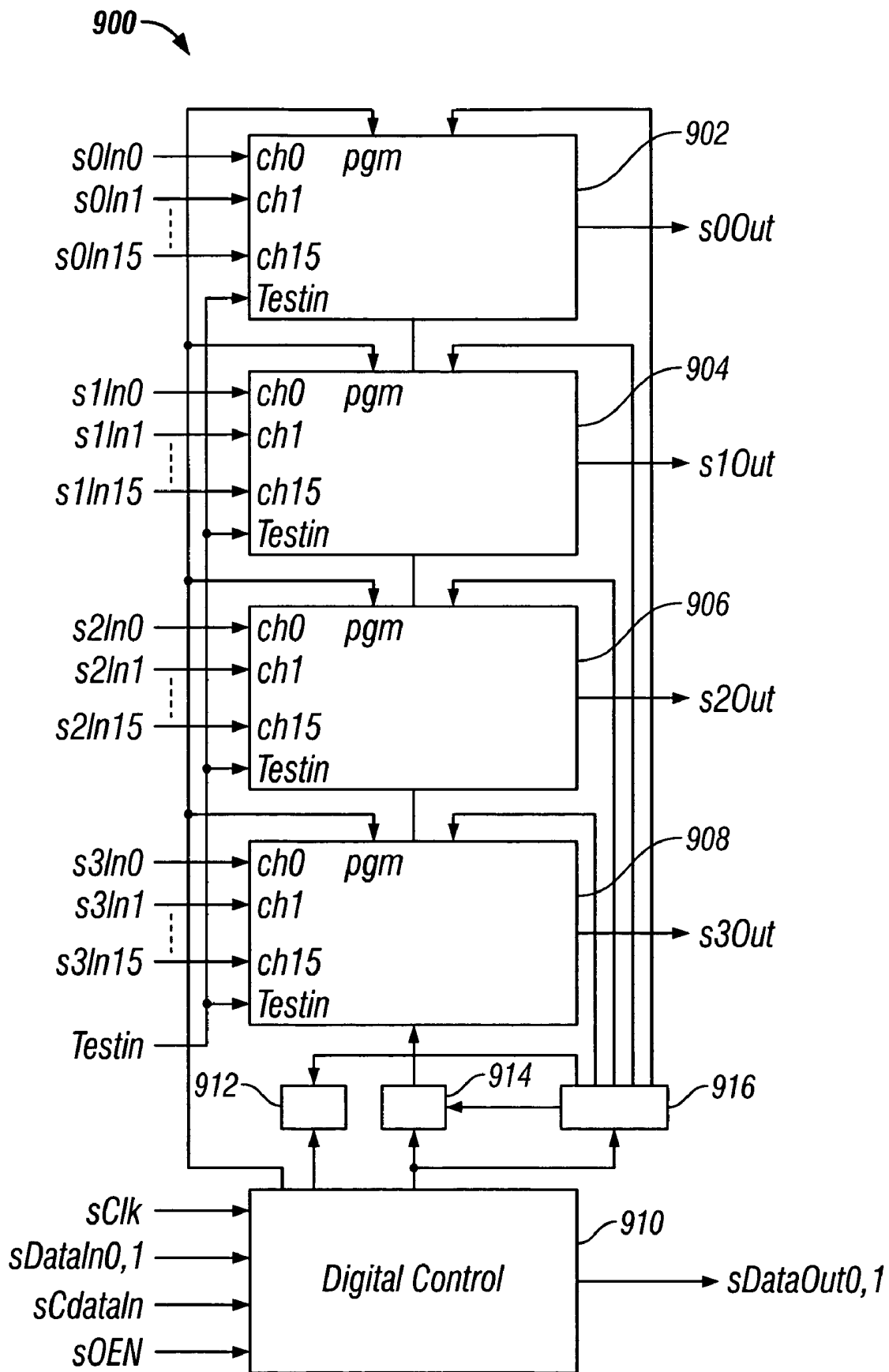
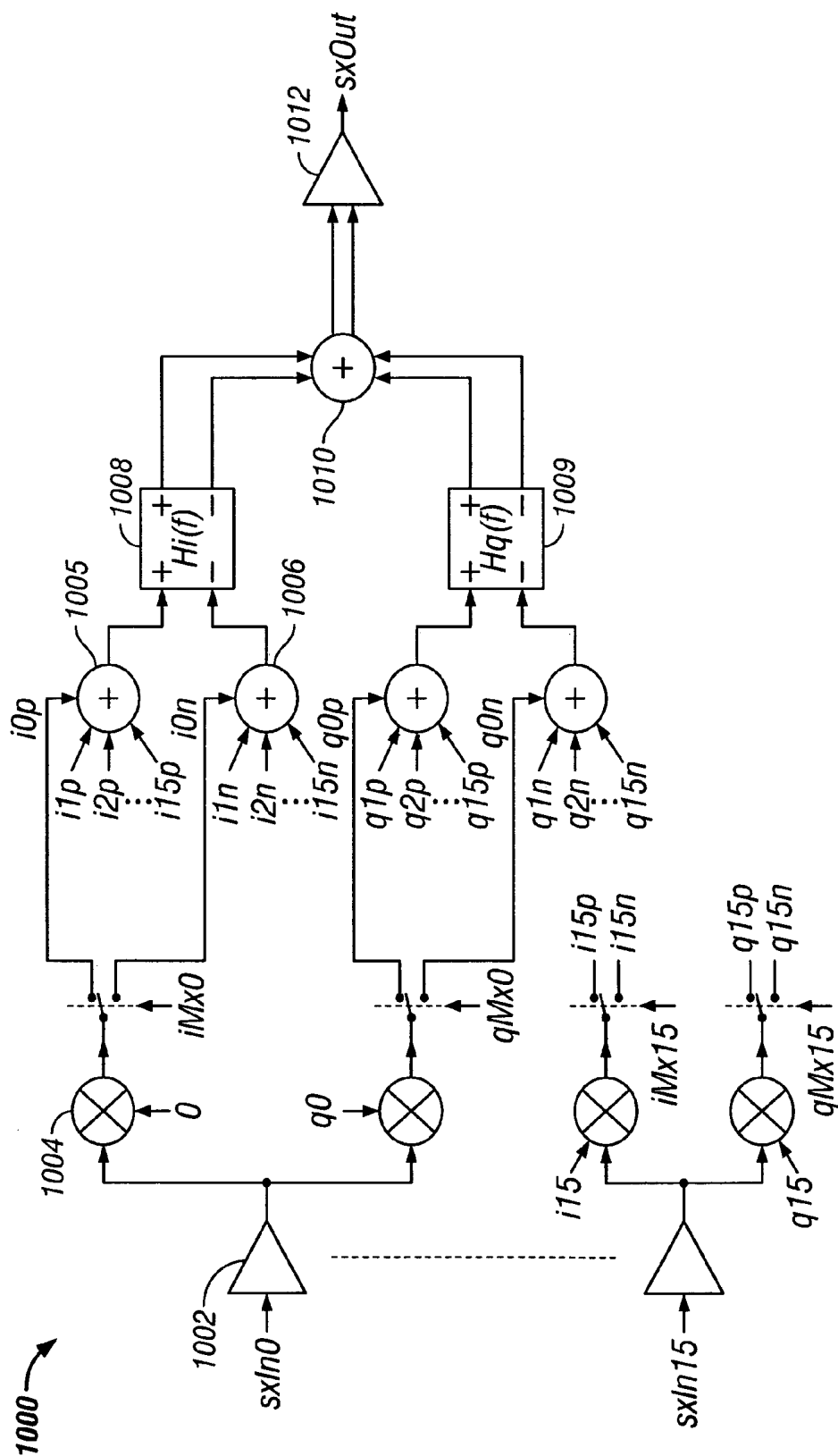


FIG. 9



Low-Noise Amplifier **Angular Weight and Sign** **First Summation** **Allpass Filters** **Second Summation** **Line Driver**

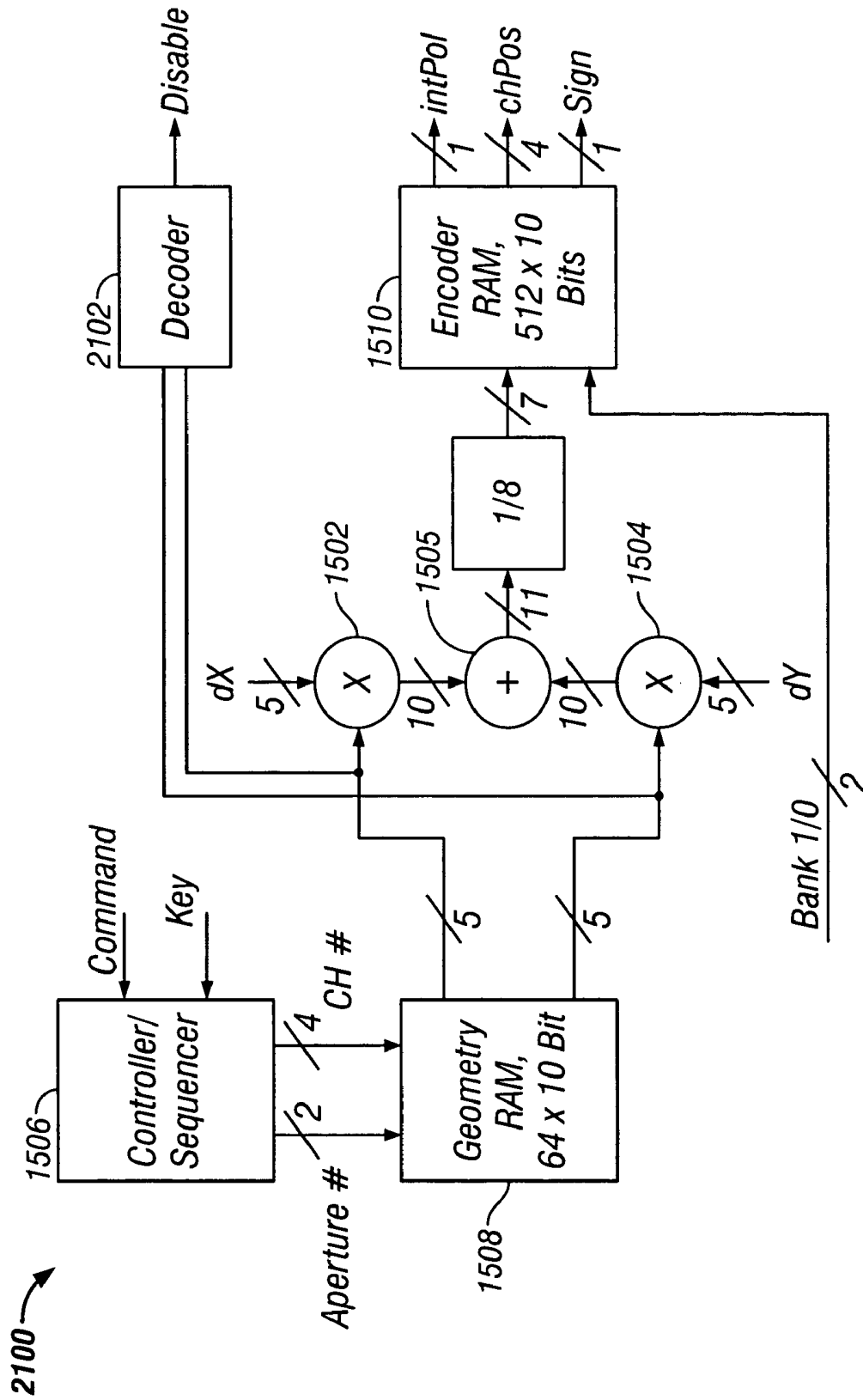


FIG. 12

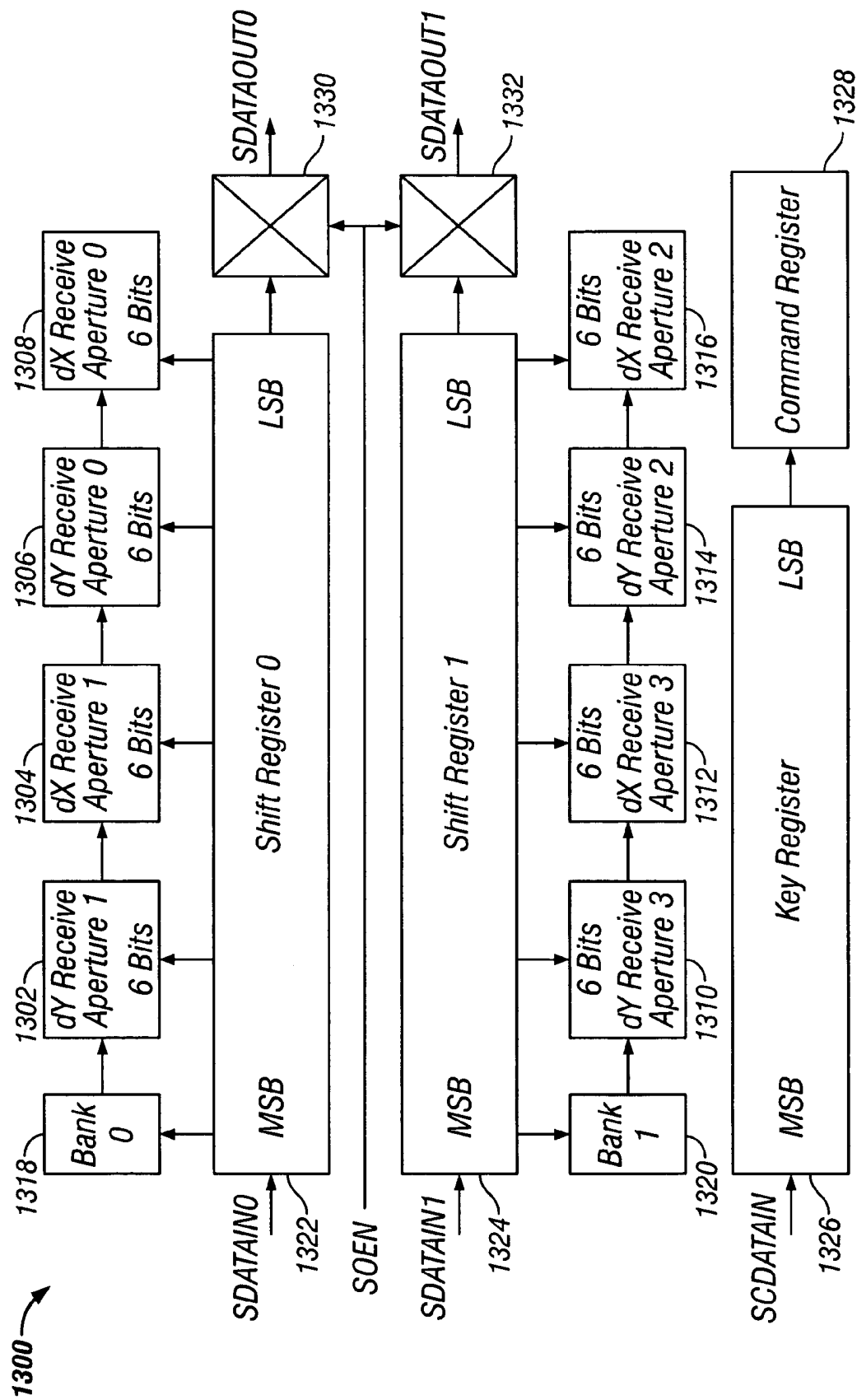


FIG. 13

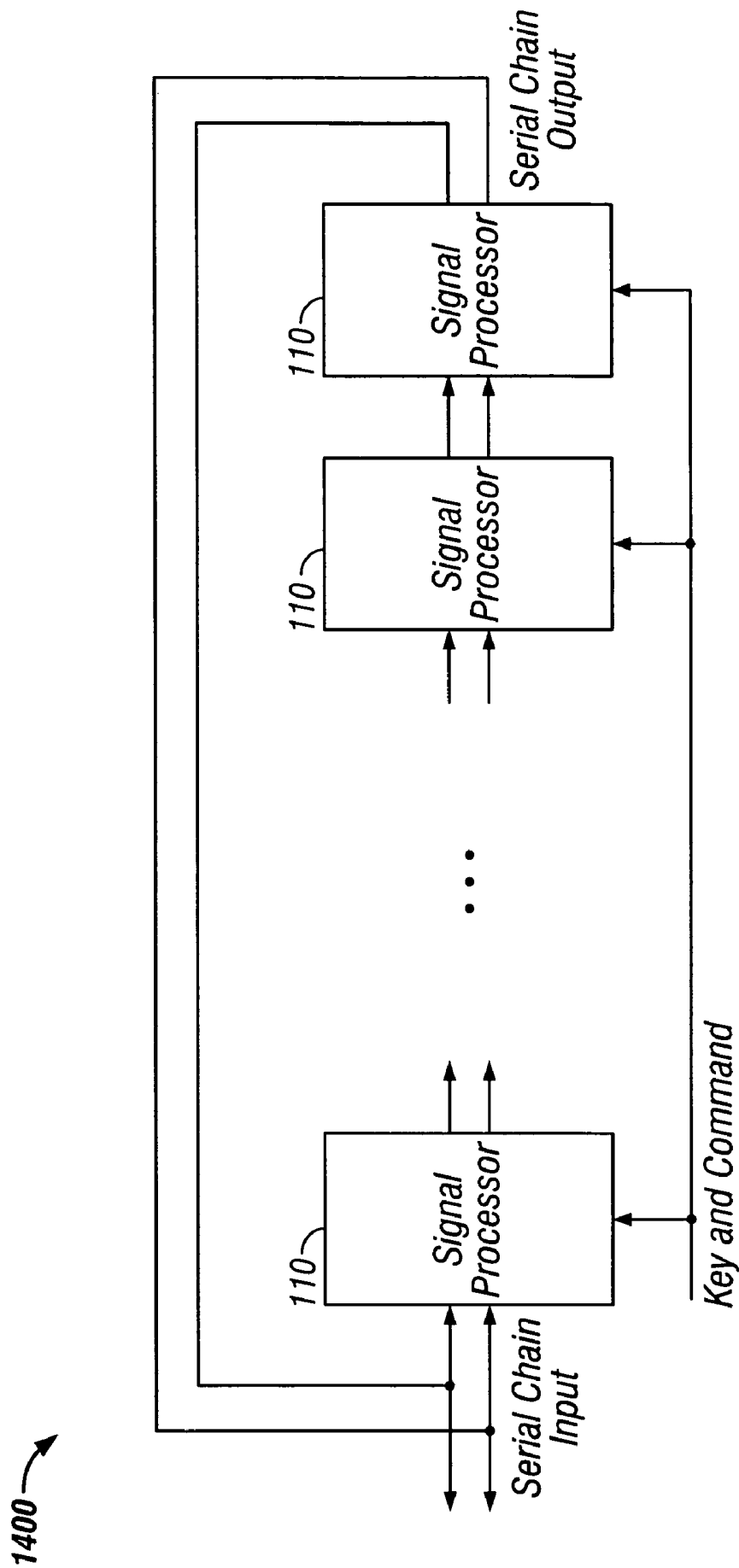


FIG. 14

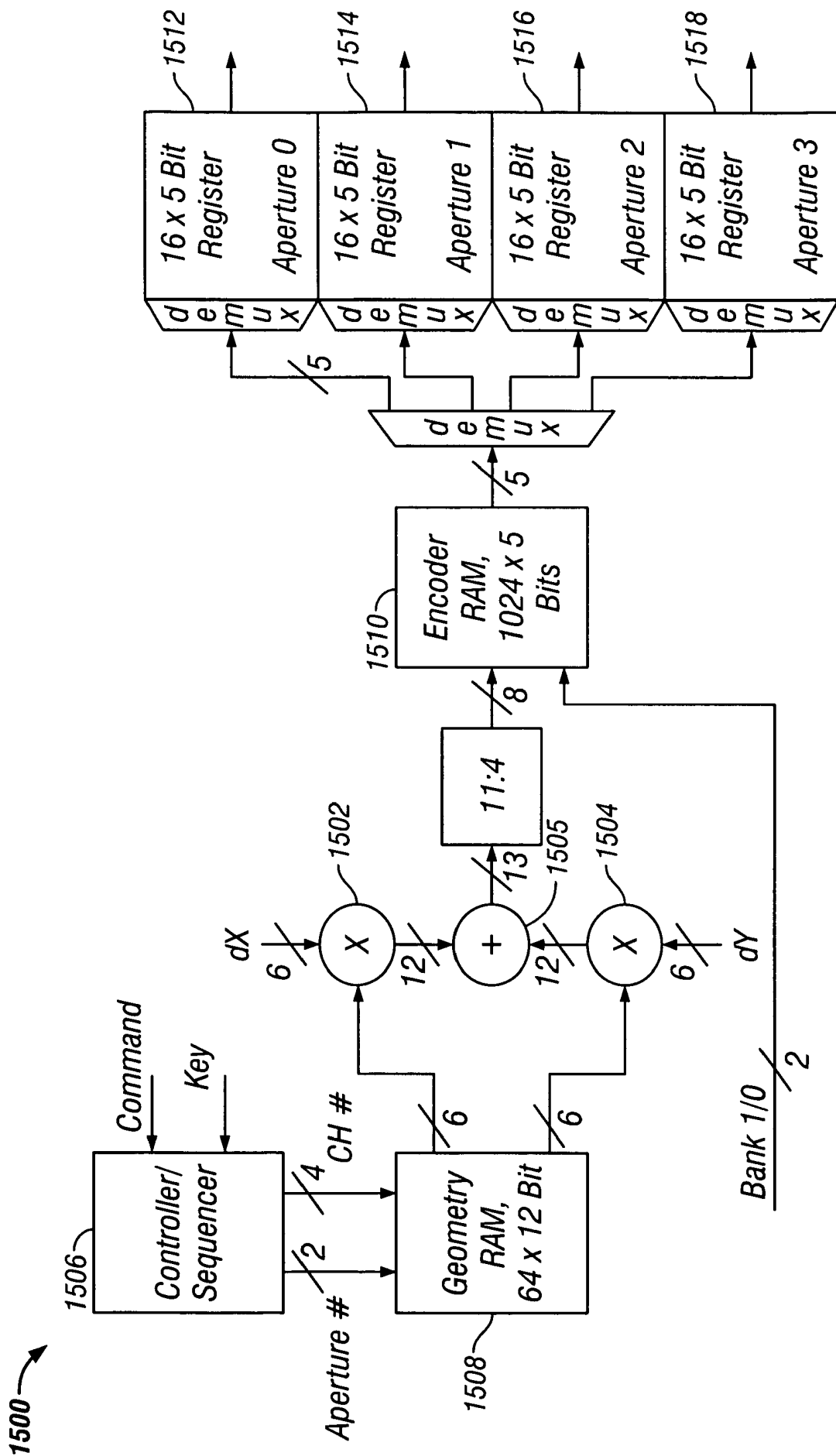
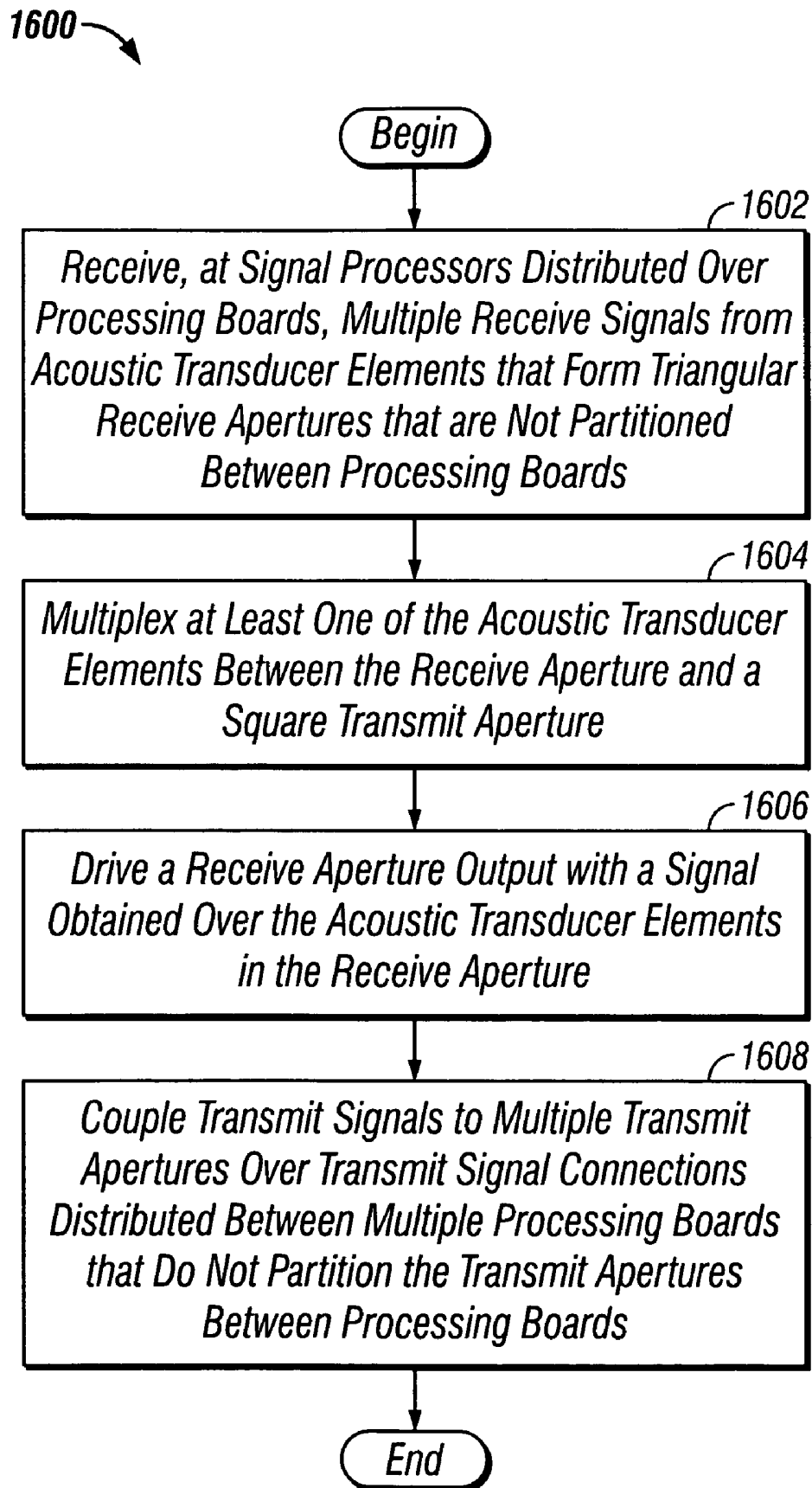


FIG. 15

**FIG. 16**

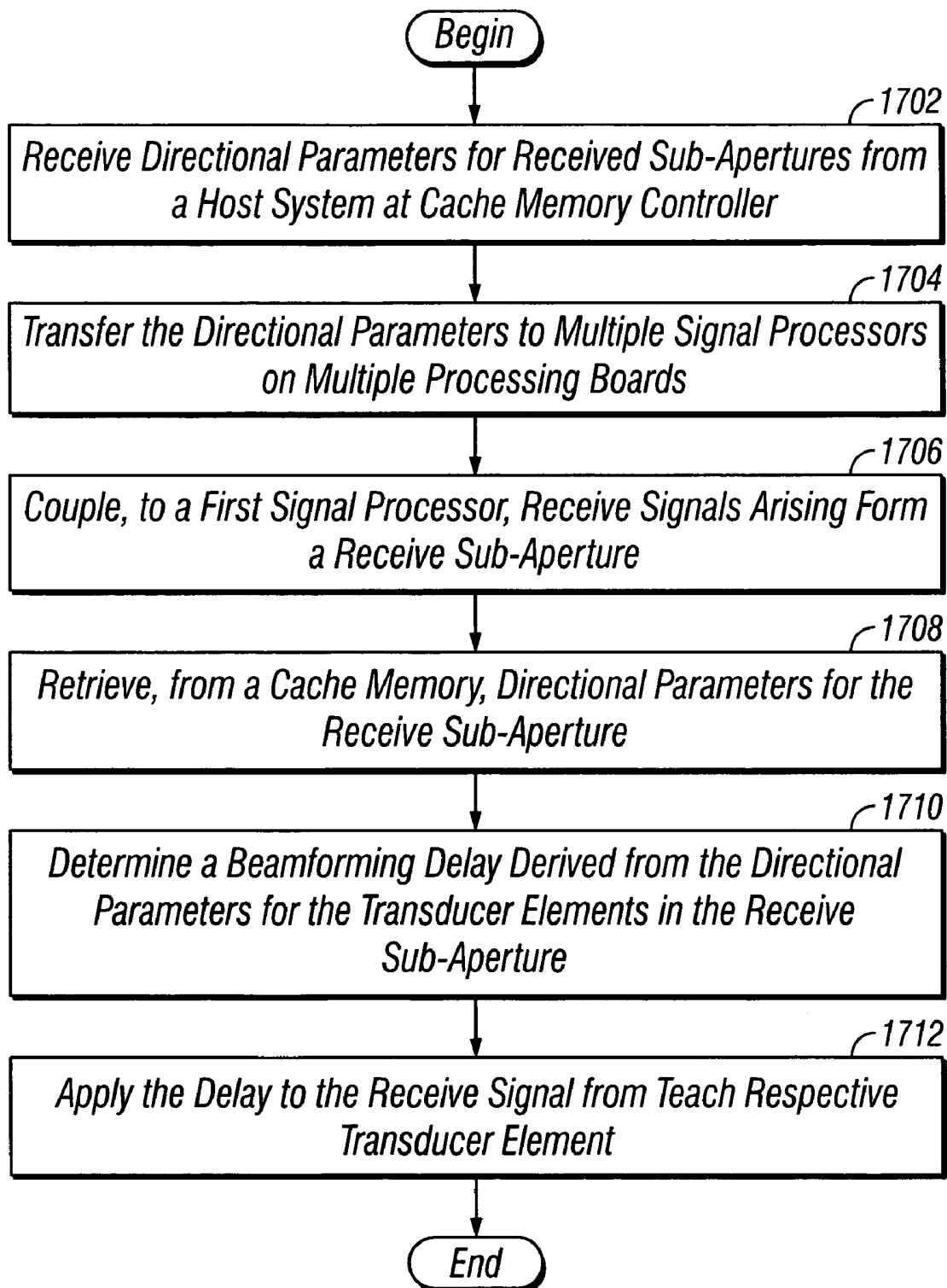


FIG. 17

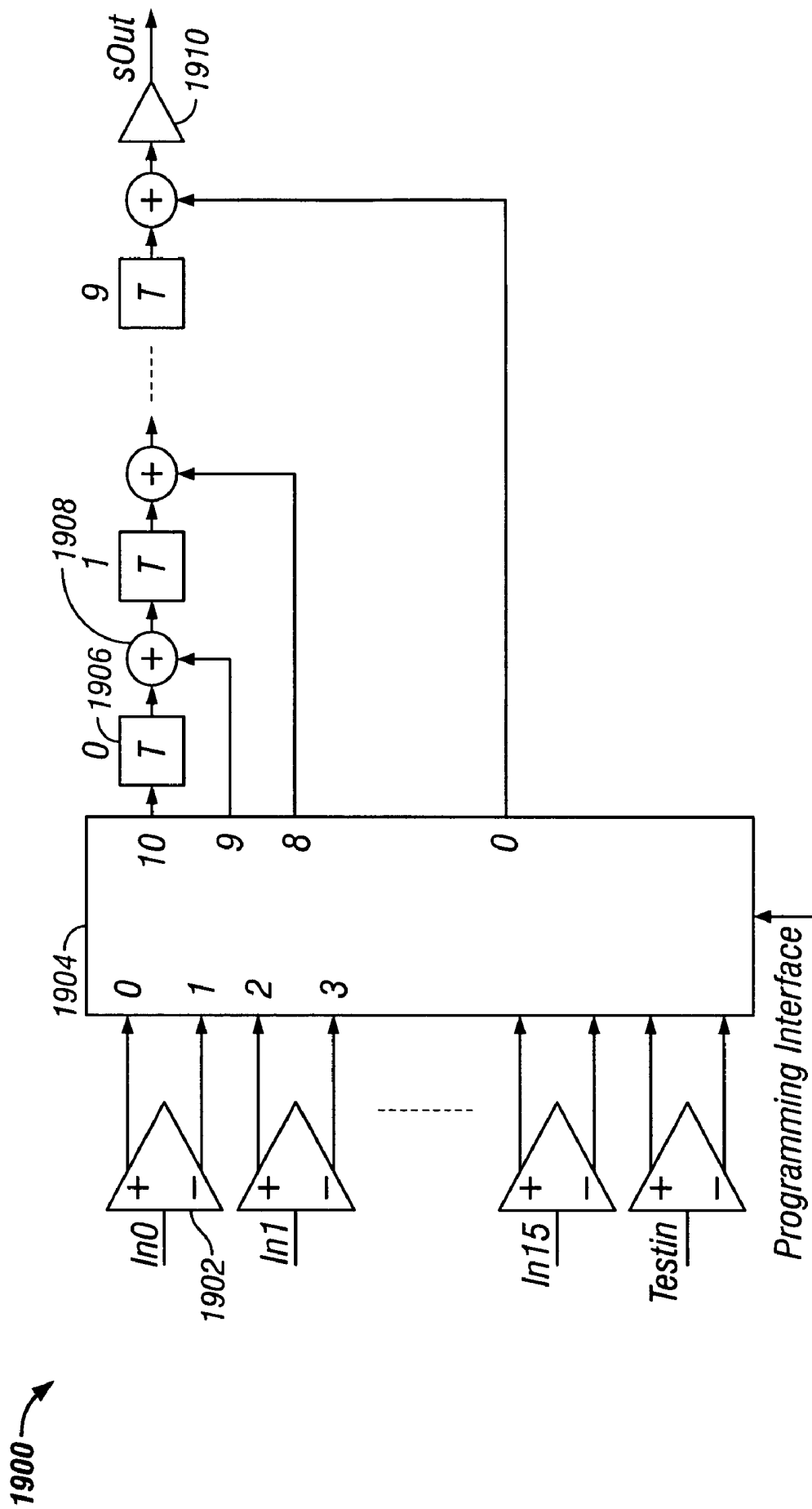


FIG. 19

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ULTRASOUND PROBE DISTRIBUTED BEAMFORMER

CROSS REFERENCE TO RELATED APPLICATIONS

This application is related to Ser. No. 10/719,531, Titled "Ultrasound Probe Sub-Aperture Processing", filed Nov. 21, 2003, and Ser. No. 10/719,431, Titled "Ultrasound Probe Transceiver Circuitry", filed Nov. 21, 2003.

BACKGROUND OF THE INVENTION

1. Field of the Invention

This invention relates generally to ultrasound medical imaging systems. More specifically, this invention relates to processing sub-apertures of a multiple element transducer probe.

2. Related Art

Doctors and technicians commonly use medical imaging systems to obtain display, and study images for diagnostic purposes. In ultrasound imaging systems, for example, a doctor may obtain images of a patient's heart in an attempt to learn whether the heart functions properly. As time moves forward, these imaging systems become increasingly adept at obtaining not only the images but also additional related diagnostic information such as ECG traces, heart rate, and the like.

Two key components of an ultrasound system are the ultrasound probe and the beamformer. The beamformer focuses and steers ultrasound energy transmitted by and received by the probe as one step in generating images of anatomic content on a display.

Development of 3D ultrasound push towards ultrasound probes with a large number of acoustic elements. Recent technology developments suggest reducing the large number of channels by sub-grouping the aperture elements and pre-process each group into one signal that is transferred to the system. Transmit can similarly be handled by transmitters solely in the probe, or by transmitting on sub-groups of the aperture.

High quality images, of course, are of great importance in clinically evaluating the physiology that a doctor is studying. High quality images require use of a non-sparse aperture, e.g., most elements on the aperture must be used both for transmit and receive. Current system, achieve this by multiplexing between the transmit and receive circuitry in the system. Each channel in the probe can then be connected with one cable to the system and be used both for transmit and receive.

The layout and implementation of the aperture sub-grouping for transmit and receive is of great importance for the image quality. The introduction of circuitry in the probe poses technical challenges that must be solved. Also, with receive and/or transmit circuitry in the probe the current approach with a transmit/receive switch in the system does not allow use off all acoustic channels on the probe for both transmit and receive.

Therefore, there is a need to overcome the difficulties set forth above and others previously experienced.

BRIEF DESCRIPTION OF THE INVENTION

In one implementation, probe located transceiver circuitry for ultrasound transducer elements includes a transmit section and a receive section. The transmit section includes a transmit section input, a transmit section output, and receive signal blocking circuitry coupled between the transmit sec-

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tion input and the transmit section output. The receive section includes a receive section input, a receive section output, and transmit signal blocking circuitry coupled between the receive section input and the receive section output. The transmit section input is coupled to the receive section output. In another implementation, the transmit section input is not coupled to the receive section output.

Other systems, methods, features and advantages of the invention will be or will become apparent to one with skill in the art upon examination of the following figures and detailed description. It is intended that all such additional systems, methods, features and advantages be included within this description, be within the scope of the invention, and be protected by the accompanying claims.

BRIEF DESCRIPTION OF THE DRAWINGS

The components in the figures are not necessarily to scale, emphasis instead being placed upon illustrating the principles of the marking systems and methods. In the figures, like reference numerals designate corresponding parts throughout the different views.

FIG. 1 illustrates a block diagram of an ultrasound probe in communication with a host system.

FIG. 2 shows a transducer stack including an array of acoustic transducer elements that may be used in the ultrasound probe shown in FIG. 1.

FIG. 3 shows receive apertures arranged across an array of acoustic transducer elements incorporated into the ultrasound probe shown in FIG. 1.

FIG. 4 depicts the transmit apertures multiplexed with receive apertures arranged across an array of acoustic transducer elements incorporated into the ultrasound probe shown in FIG. 1.

FIG. 5 shows a distribution of forty-eight (48) transducer flex cables connected to eight (8) processing boards for connecting the array of acoustic transducer elements in the probe to signal processor on the processing boards.

FIG. 6 illustrates transceiver circuitry for multiplexing selected acoustic transducer elements between reception and transmission, while protecting the signal processors connected to the acoustic transducer elements.

FIG. 7 illustrates one embodiment of transceiver circuitry using passive circuitry for multiplexing selected acoustic transducer elements between reception and transmission, while protecting the signal processors connected to the acoustic transducer elements.

FIG. 8 shows the front side and the back side of a processing board, including suggested layout areas for the electronics carried by the processing board.

FIG. 9 depicts a block diagram of a signal processor suitable for use with the ultrasound probe shown in FIG. 1.

FIG. 10 shows narrowband beamforming circuitry in the signal processor.

FIG. 11 shows an all-pass filter cell.

FIG. 12 shows a second implementation of a cross-point controller.

FIG. 13 shows a block diagram of a digital interface for the signal processor.

FIG. 14 shows signal processors connected in a serial chain.

FIG. 15 shows a cross-point controller in the signal processor that calculates new control values for processing the four receive sub-apertures assigned to the signal processor.

FIG. 16 shows steps that the ultrasound probe shown in FIG. 1 may take to perform sub-aperture processing.

FIG. 17 illustrates steps that the ultrasound probe shown in FIG. 1 may take to perform beamforming in the probe.

FIG. 18 shows steps that the ultrasound probe shown in FIG. 1 may take to transmit and receive energy to an acoustic transducer element multiplexed between a receive aperture and a transmit aperture.

FIG. 19 shows another implementation of beamforming circuitry for the signal processors.

DETAILED DESCRIPTION

FIG. 1 illustrates a block diagram of an ultrasound probe 100. The probe 100 includes a transducer array and backing stack 102 (the "transducer array 102"), transducer cables 104, and multiple processing boards 106 that support processing electronics. Each processing board 106 includes a memory 108 (which may include geometry RAM, encoder RAM, location registers and control registers as noted below) and signal processors 110. A location cache memory and controller 112 (e.g., a general purpose CPU, microcontroller, PLD, or the like) is also present and includes a communication interface 114. The memory 108 may be separate or included as part of the signal processor 110.

The communication interface 114 establishes data exchange with the host system 116 over the digital signal lines 118 and through the signal cable 120. In addition, the signal cable 120 includes coaxial cables 122 that connect to the processing boards 106 to carry transmit pulse waveforms to the transducer array 102 and to carry back receive signals, after beamforming, to the host system 116. In another implementation the coaxial cables 122 only carry receive signals. The probe 100 may include the connector 124, through which the probe 100 attaches to the host system 116.

An interconnection 126 may be provided to connect the transducer flex cables 104 to the processing boards 106. The interconnection 126 thereby establish electrical connectivity between the transducer flex cables 104 and the processing boards 106. The interconnection 126 may be a connector, although other implementations are also suitable.

The transducer array 102 is bonded onto the backing stack, as will be described in more detail below with regard to FIG. 2. The transducer flex cables 104 provide electrical signal connections through the backing stack. In one embodiment, there are forty-eight (48) transducer flex cables 104, each with fifty-five (55) signal connections. Thus, the transducer flex cables 104 support transmit and receive signal connections for as many as 2640 transducer elements in the transducer array 102, although fewer are used in the implementation described below.

The interconnection 126 connects the transducer flex cables 104 to the processing boards 106. In one implementation, each processing board 106 couples to six planes of transducer flex cables 104, and thereby includes signal connections for 330 transducer elements.

The processing boards 106 may, like the flex cables 104, be formed from flex material. The processing boards 106 hold the processing electronics for the transducer array 102, including the signal processors 110 that perform beamforming on the receive apertures in the transducer array 102. The processing boards 106 also hold the transceiver circuitry for multiplexing selected acoustic transducer elements between reception and transmission, while protecting the signal processors 110 connected to the acoustic transducer elements.

As will be described in more detail below, each signal processor 110 may handle plural receive sub-apertures, for example four, defined at selected spatial locations on the transducer array 102. The receive sub-apertures may be tri-

angular sub-apertures that include fifteen (15) acoustic transducer elements arranged, for example, as a row of five elements above a row of four elements above a row of three elements above a row of two elements above a row of one element. Furthermore, each processing board 106 may include six (6) signal processors. Thus, in the receive direction, each processing board 106 may process up to twenty (24) receive sub-apertures, each including fifteen acoustic transducer elements.

For every ultrasound beam, the cache memory and controller 112 connects over digital signal lines 133 (e.g., carried by a separate flex cable) to each signal processor controller 108 on each processing board 106. The signal processor controller 108 are drawn as a separate block labeled 'memory' on the processing board 106, but may also be included as part of the signal processor 110. The cache memory and controller 112 transfers static and dynamic probe setup information to the signal processor 110. Static setup information is typically spatial element locations, power settings, and delay setting mapping tables. Dynamic information is typically directional information for the sub-apertures that vary from beam to beam. The digital signal lines may include, for example, a clock line for each processing board 106, a serial command data line for each processing board 106, one or more data lines connected to each processing board 106, an output enable for one or more of the signal processors 110, and a test signal.

The cache memory and controller 112 communicates with the host system 116 over the digital signal lines 118 that may form part of a synchronous serial port, for example. To that end, the communication interface 114 and digital signal lines 118 may implement a low voltage differential signal interface, LVDS, according to the TIA/EIA-644 and IEEE 1592 standard, for example, including a coaxial cable with a grounded shield and center signal wire. The cache memory and controller 112 includes a block of cache memory 132, for example, 1-64 MBytes of static random access memory (SRAM).

The main purpose of the cache memory 132 in the cache memory and controller 112 is to keep beam dependent setup information for the sub-apertures. In one implementation this may be directional setup information for the sub-apertures. This is typically divided into pages where each page contains the signal processor 110 setup information required in relation to each shot. By loading up the cache pages with information for all shots in a scan sequence, this information is available in the probe during scanning. During scanning the probe setup information in relation to each shot can then be made available to the signal processors by transferring the relevant cache memory pointer to the cache memory and controller 112.

In one implementation, the cache memory 132 in the cache memory and controller 112 is organized into of 512 k words $\times$ 16 bit (8 Mbit) and divided into pages of 128 words. The cache memory pointer can be set to the start of each page. The cache memory pointer may be, for example, a 12 bit pointer that may address a total of 4096 pages. When the cache memory 132 is a 4 Mbit cache, the cache memory pointer may be an 11 bit pointer to index 2048 pages. The words of a cache page are employed when writing or reading data to or from a chain of signal processors 110. The digital data lines for the signal processors 110 on each processing board may be chained through shift registers over a series of plural signal processors 110. Thus, data transferred to the signal processors 110 propagates serially through the signal processors 110. The bit from the word with the lowest address in a page will end in the LSB bit of the shift register to the last signal processor 110 in a chain when loading data. Further,

the cache memory **132** is shown within the cache memory and controller **112**, but in alternate implementations the cache memory **132** may be separate from the cache memory and controller **112**. The cache memory may also be part of the signal processors **110**.

The probe **100** response to e.g. sixteen bit commands from the host system **116**. One exemplary set of commands is shown below in Table 1. Four bits in the command may be used to define the command, while twelve bits may be used as parameters for the command.

TABLE 1

Name	Parameters Bit: 11-0	Description	Details
WR_CTRL__REG	control registry setting	Write to control/status register	cache memory and controller register
WR__CACHE__PTR	11/12 bit pointer	Set cache page pointer	The cache pointer indicates the start of the next page which will be loaded from cache memory and into the signal processors 110 . The address pointer might be automatically incremented For each word written.
WR__CACHE		Write a page from the host system 116 to the cache memory 132 .	
LD__SCAN__PAR		Write scan parameter page to signal processor 110 chain.	Updated for each ultrasound shot.
LD__CONFIG		Load memories or registers in the signal processors 110 .	Static configuration data.
DELAY__TUNE	None	Start delay calibration	Each signal processor 110 has an internal circuit to calibrate the delays
SAP__RESET	What to reset		
RD__CTRL__REG	Control register value returned	Read from control/status register	This register is internal to the cache memory and controller 112 .
RD__CACHE__PTR	Pointer value returned	Read cache page pointer register	Useful for test and verification.
RD__CACHE	None	Read a page from cache memory 132 .	The address pointer might be automatically incremented for each page read.
RD__CONFIG		Read setup from signal processor 110 .	E.g. through loop back from last signal processor 110 in chain.
CMD__ENABLE	ID code	To enable and disable command execution.	

The purpose of the command set is to control the probe. The commands may control the cache memory and controller **112** and/or the signal processors **110**. It is also desirable to include a protect mechanism to avoid undesired command execution due to noise, e.g. from the transmit pulses.

The Write Cache Pointer (WR__CACHE_PTR) command writes to the memory cache pointer register. In one implementation the parameter is a 12 bit cache pointer. The specified cache pointer is employed in the parameter field of the command when reading/writing the cache memory **132**. During read/write of cache words the cache pointer might be

automatically incremented. After transfer of a full page, the pointer will thus point to the start of next page. If more than 8 MBit are used, transfer of a longer cache pointer than 12 bit can be implemented as two commands.

The Write to Cache (WR__CACHE) command loads data into the cache memory **132**. Data will be written to the cache page pointed to by the cache pointer. The cache pointer is automatically incremented after each word written to the cache. The location memory controller **112** may send a command echo when this command is received.

The Load Scan Parameters (LD__SCAN_PAR) command writes scan parameters to the signal processor **110** chain. The parameter, in one implementation, is not used. This command writes a scan parameter page to signal processors **110** from the cache page given by the cache address pointer. This command may be triggered by the EOL signal, but may also be sent as a command.

When the data is transferred, the cache memory and controller **112** sends a calculate command to the signal processors **110** to initiate calculation of beamforming delays for the next ultrasound shot (using previous loaded setup values to save setup time). The cache memory **132** pointer is automatically incremented after each word that is written to the signal processors **110**. The size of a scan parameter page may be, for example, 128 words. The word with the lowest address will end up in the LSB bit in the shift register in the last signal processor **110** in a chain.

The Load Configuration (LD__CONFIG) command loads the static setup information to the signal processor **110**. Static setup information is typically spatial element locations, power settings, and delay setting mapping tables inside a signal processor **110**. Each time the command is used one cache page is written to the selected memory. Some loads may require more than one cache page.

Within the signal processor the Geometry RAM holding the spatial element location may be implemented as 64 words, each 12 bits in length. The Encoder RAM holding the delay-mapping table may be implemented as 1024 words, each 5 bits in length. The start address is taken from cache memory **132** address pointer. After each page, the address pointer is incremented to next cache page. Subsequent pages may thus be loaded without updating the address pointer. The word with the lowest address in a page is the first data clocked into the signal processor **110** chain. Thus, the content of the lowest address will end up in the LSB bit of the shift register of the last signal processor **110** in the chain of signal processors **110** on a particular processing board **106**.

The Initiate Delay Tuning (DELAY__TUNE) command initiates the process of calibrating the internal delays in the signal processors **110**. The parameter need not be used. The result is written to the analog multi-purpose register present in the signal processor **110**.

The SAP Reset Command (SAP__RESET) command resets all the internal functions or address counters in a signal processor **110**. The parameter may specify a bit pattern that selects between resetting the entire signal processor **110** or sub functionality only.

The Read Control Register (RD__CTRL__REG) command reads the control register inside the location memory controller **112**. The register content may be returned in the parameter field of the command.

The Read Cache Pointer (RD__CACHE_PTR) command reads the cache memory **132** pointer register. The value read from the cache pointer register may be returned in the parameter field of the command before the command is echoed back to the host system **116**.

The Read Cache (RD_CACHE) command reads data from the cache memory **132** to the host system **116**. Once the command is received the location memory controller **112** may send data words as a continuous sequence of words.

The Read Configuration from SAP (RD_CONFIG) command reads configuration data from the signal processors **110** specified by the parameter bits Configuration data is read from the signal processors **110** and placed in the cache memory **132** in the cache page pointed to by the cache pointer. The cache address is incremented for each word read. The first word is placed in the lowest cache address. The cache address is adjusted to the start of next page when finished.

The Command Enable (CMD_ENABLE) command enables or disables command execution. After loading of scan parameters from the cache memory **132** command execution is disabled after the command is finished. Nevertheless, while disabled, the location memory controller **112** may still respond to the command enable command and the read control register command. A unique bit pattern may be added to the parameter field to reduce the possibility for this command to be generated from noise present on the command line.

As an overview, the following steps occur during scanning. First, an EOL signal (end of receiving data from previous ultrasound shot) triggers the cache memory and controller **112** to send a calculation command to signal processors **110**, then transfer of a new page from the memory cache **132** to the signal processors **110**. A page pointer register in the cache memory and controller **112** holds the start address for this new page. Prior to each upload the system host **116** sends the page pointer for the next ultrasound shot down the digital signal lines **118** to the cache memory and controller **112**. When the page load is finished, an acknowledge signal might be sent back to the system host **116**. The system host **116** then fires the ultrasound shot and acquisition of ultrasound data continues. When acquisition of the current shot is finished, the location memory controller **112** receives a new EOL and the process starts over again.

When the probe **100** is connected to the host system **116**, the host system **116** transfers the setup information for each aperture and each beam into the SRAM on the location memory controller **112**. The receive beamforming is split between the host system **116** and the probe **100**. The host system **116** is responsible for the beamforming delay, aperture expansion, and amplitude apodization of the system receive channels driven by the signal processors **110** on the receive aperture outputs.

The signal processors **110** perform the beamforming on the individual receive sub-apertures. In one implementation, groups of fifteen transducer elements, arranged as triangular receive sub-apertures, are coupled to the signal processors **110**. The signal processors **110** apply a delay to each of the receive signals arising from each of the transducer elements. The signal processors **110** also add the fifteen receive signals together and drive the aperture sum back to the host system **116** over the receive aperture outputs and the coaxial cables **122**.

In one implementation using phase delays, each signal processor **110** includes, for each receive sub-aperture, fifteen (15) low noise amplifiers, fifteen (15) phase inverters, a capacitor switching network, and a two phase shifter that applies a 90 degree differential phase shift. In this embodiment the differential phase shift is wideband. The switching network applies weighting factors to the potentially inverted receive signals for summation into the phase shifters. In another implementation the signal processor are based on a delay line chain.

During operation, each signal processor **110** is configured so that the beamsteering for each receive sub-aperture points toward a focal point selected by the host system **116**. To this end, the signal processor **110** determines the beamforming phase shifts based on the transducer element position within the receive aperture, the steering direction, and the receive frequency. Note that each receive sub-aperture need not use the same focal point and that receive sub-apertures farther away from the center of the transducer array **102** may be turned on later to achieve dynamically increasing aperture sizes.

The configuration of the signal processor **110** occurs in two steps. First, during probe **100** initialization, the host system **116** loads static signal processor setup information via the cache memory and controller **112** into the signal processor **110**. This static information includes the geometry information, i.e., the spatial (x,y) location of the transducer elements in each receive sub-aperture and a frequency dependent translation table. Second, prior to scanning the dynamic setup information is transferred to the cache memory **132** in the cache memory and controller **112**. Each one of these cache pages contains steering parameters for all sub-apertures in the probe in relation to one shot. In another implementation more than one cache page could be used to transfer the required beam related setup information.

During scanning, the host system **116** provides a beam index to the cache memory and controller **112**. In response, the cache memory and controller **112** transfers the appropriate steering parameters from its cache memory to the signal processors **110**. The signal processors **110** then determine beamforming delays based on the transducer element positions, the steering direction (as represented by the direction parameters). For the implementation using phase delays, the delays are converted to phase settings using the frequency dependent translation table.

Turning next to FIG. 2, that figure shows one implementation of the transducer array **102**. The transducer array **102** includes piezoelectric ceramic **202** that converts electrical-to-acoustic and acoustic-to-electrical energy. The piezoelectric ceramic **202** is located within the center of the transducer array **102**. On the signal side, the piezoelectric ceramic **202** is attached to a z-axis backing layer **204** with transducer flex cables **104**.

The transducer flex cables **104** provide for high density signal connection. The ceramic **202**, an electrically conductive inner acoustic matching layer **210**, and the top surface of the backing block **204** form discrete acoustic elements **212** centered over each of the flex circuit traces **206** in the transducer flex cables **104**. Thus, there is a signal plane **213** on the z-axis backing block **204**.

Each circuit trace **206** contacts the bottom, or signal side, of one transducer element **212**. This diced matching layer **216** is attached to the top of each element **212** to form a ground connection across the transducer array **102** face.

With regard next to FIGS. 3 and 4, FIG. 3 shows receive sub-apertures arranged across an array of acoustic transducer elements **300** incorporated into the ultrasound probe shown in FIG. 1. Similarly, FIG. 4 shows the transmit sub-apertures for one row, multiplexed with certain receive apertures arranged across the array of acoustic transducer elements **300**. The other rows shown also contain transmit elements. In one embodiment, the array includes 55 transducer elements in the lateral direction and 48 elements in the elevational direction.

However, in the implementation described below, the corners of the array are omitted which gives the array **300** an octagonal shape. All of the transducer elements, grouped into fifteen element receive sub-apertures, are used in the receive

direction as shown in FIG. 3. All transmit elements, grouped into four element transmit sub-apertures are also used in the transmit direction as shown in FIG. 4.

With reference specifically to FIG. 3, each signal processor 110 combines the fifteen receive signals arising from the fifteen transducer elements for each receive sub-aperture into a single system receive channel. The signal processor 110, as noted above, applies a delay to each receive signal before summing the receive signals. The groups of 15 transducer elements form triangular apertures as indicated in FIG. 3. Thus, the overall transducer receive aperture includes 160 sub-apertures including $160 \times 15 = 2400$ transducer elements. In other embodiments, the numbers of receive sub-apertures and the numbers of transmit sub-apertures chosen depend on the number of system channels available for transmit and receive, the desired aperture size and shape and the transducer elements size.

As shown in FIG. 3, with respect to the enlarged receive aperture 48, each receive aperture is formed on a 5 by 5 grid of transducer elements. The receive aperture includes a first row of five transducer elements (labeled 11-15), a second row of four transducer elements (labeled 7-10), a third row of three transducer elements (labeled 4-6), a fourth row of two transducer elements (labeled 2-3), and a fifth row of one transducer element (labeled 1). Each transducer element has a location x_n, y_n within its sub-aperture. For example, transducer element 14 is located at $x_n=3, y_n=0$. The receive apertures are interlocked such that the combination of two receive apertures forms a rectangular patch of 5 transducer elements in lateral and 6 transducer elements in elevational direction.

With respect to FIG. 4, the shown part of the transmit aperture includes 324 transducer elements along the fifth (5) row of receive elements of the array 300. The transmit elements are grouped into 2×2 element transmit sub-apertures and each one of the transmit sub-apertures is connected to one of the system transmit channels that are carried back to the host system 116 on the coaxial cables 122. FIG. 4 shows the transmit sub-aperture 168 enlarged, including a first row of two transducer elements (labeled 3-4) and a second row of two transducer elements (labeled 1-2). The staggering of the transmit sub-apertures in the lateral (horizontal) direction is done to reduce transmit grating lobes.

In the elevation direction, three of the 2×2 transmit sub-apertures are aligned with six receive transducer elements. In the elevation (vertical direction) the overall array 300 is divided into eight groups of six rows of transducer elements each. The arrangement of the transmit and receive sub-apertures sets up the electronics partitioning. More specifically, each group of six element rows (e.g. the one labeled a-f in FIGS. 3 and 4) is connected to one processing board 106 by six transducer flex cables 104. Because no receive sub-aperture or transmit sub-aperture crosses over the partition boundary (onto two or more processing boards), the processing electronics associated with every transducer element in the six rows are entirely contained within a single processing board 106. One significant advantage is that there is no need to route analog signals from one processing board 106 to another.

FIG. 5 illustrates a distribution 500 of forty-eight (48) transducer flex cables 104 emerging from the backing stack 204 of the transducer array 102. Six transducer flex cables 104 connected to each of eight (8) processing boards 106. The transducer flex cables 104 thereby connect the array 300 of acoustic transducer elements to the signal processors (two of which are illustrated as elements 110) on the processing boards 106. Spacers 504 may be placed in between the processing boards 106 to give desired spacing.

Each transducer flex has a connection that provide signal paths for fifty-five (55) transducer elements to connect to a particular processing board. To that end a connector is provided to couple the signals from the transducer flexes 104 to the processing board 106. There are eight such processing boards 106 in the implementation described in this document. Thus, eight processing board 106, as indicated in FIG. 5, are stacked to create a complete distribution of forty-eight transducer flex cables 104 to the processing boards 106.

FIG. 6 shows a probe circuitry for multiplexing selected acoustic transducer elements between reception and transmission, while protecting the probe electronics for transmit and receive. The implementation 600 uses the coaxes 606 to the system for both transmit and receive. In this implementation the probe receive processing circuitry 604 must have protecting circuitry both on input 603-604 connection, and on its output 602-604 connection. In another implementation with transmit circuitry in the probe 601, only the receive circuitry input, the 603-604 connection, must be protected. In this implementation the transmit circuitry need are controlled from the system over the lines 608, or from the probe cache memory and controller 112.

The multiplexing circuitry 602 and 603 may be implemented using switches or passive circuitry. An embodiment with active switches, the control circuitry must be timed relative to the signal flow. An embodiment using passive circuitry, as shown in FIG. 7, is protecting the probe circuitry based on the signal levels only. For all embodiments the multiplexers or switches used must withstand the high voltage transmit voltage, typically in the range from 10 to 400 volt peak-to-peak for piezoelectric transducer elements. For other types of transducer elements, other voltage ranges may be used.

FIG. 7 shows a passive implementation of a transceiver circuitry 700 for multiplexing selected acoustic transducer elements between reception and transmission, while protecting the signal processors connected to the acoustic transducer elements. The transceiver circuitry 700 includes multiple transmit sections, one of which is labeled 702 that incorporates a transmit section input 704, a transmit section output 706, and the two sets of receive signal blocking circuitry disposed between the transmit section input 704 and the transmit section output 706. As shown in FIG. 7, the receive signal blocking circuitry includes the back-to-back diode D1; and the back-to-back diode D3 coupled to the capacitor Cshunt.

The transceiver circuitry 700 also includes multiple receive sections, one of which is labeled 708 that incorporates a receive section output 710, a receive section input 712, and two sets of transmit signal blocking circuitry disposed between the receive section input 712 and the receive section output 710. The transmit signal blocking circuitry includes the capacitor Ccoupl connected to the diode D2; and the back-to-back diode D4 connected to the capacitor C2. The receive section inputs 712 are receive signal connections that transport receive signals obtained from the transducer elements to the signal processor 110.

The acoustic transducer elements are coupled to the transmit section output 706 and the receive section input 712. The transmit section output 706 and the receive section input 712 are connected together at the transducer elements, one of which is labeled E in FIG. 7. Similarly, the transmit section input 704 and the receive section output 710 are connected together. The receive section output 710 acts as a receive sub-aperture output driven by the signal processor 110 in the receive direction. The receive sub-aperture output thus carries a signal obtained over a receive sub-aperture, for example, a

beamformed receive signal formed from receive signals obtained from 15 transducer elements in a triangular receive sub-aperture.

Note that each transmit section **702** is coupled to four transducer elements **E** through four diodes **D1**. The four transducer elements form the 2x2 transmit sub-aperture explained above. Similarly, fifteen transducer elements **E** are combined and summed into one receive sub-aperture output channel. Each of the fifteen receive section inputs **712** for a given receive sub-aperture includes the capacitor C_{coupl} and diode pair **D2**. On the output side, each of the receive section outputs **710** for the combined signal obtained over the receive sub-aperture includes the diode pair **D4** and the capacitor **C2**.

The transceiver circuitry **700** permits the transducer elements **E** to be multiplexed between signal reception and signal transmission while protecting the inputs and outputs of the signal processor **110**. In other words, any given transducer element **E** may be employed to both transmit acoustic energy and receive acoustic energy.

It might not be desirable to multiplex every transducer element **E**, however. If some of the transducer elements in the array **300** are used for reception only, a transducer element **E** need not have a transmit section **702** coupled to it. This is shown in FIG. 7 and the receive only elements labeled **714** and **716**. Furthermore, the transmit signal blocking circuitry may be omitted for a receive only transducer element. Similarly, a transducer element **E** employed only in the transmit direction need not have a receive section **708** coupled to it, nor include the receive signal blocking circuitry. Thus, for example, the receive signal blocking circuitry labeled **718** (as well as C_{coupl} and **D2**) may be omitted for a transmit only channel.

In operation, the transmit signal (e.g., a 100 volt pulse) coming from the host system **116** passes through the diodes **D3**, the tuning inductor L_{tuning} and the diodes **D1** to drive the transducer elements **E**. After the tuning inductor, the transmit signal splits into four signals and passes through four sets of **D1** diodes to the four transducer elements that make up a 2x2 transmit sub-aperture.

As shown in FIG. 7, the diodes **D1**, **D2**, **D3**, **D4** appear as antiparallel pairs. The voltage drop on the diodes is small compared to the transmit voltage and do not have a significant impact on the transmit signal during transmit. The tuning inductor is selected to provide a voltage step-up to the transducer elements **E**. The resonance frequency of that circuit (i.e., the tuning inductor and the effective capacitance) is tuned to match the desired transmit frequency. The effective capacitance is formed by the parallel components of transducer element, the parasitic shunt capacitance and the coupling capacitor C_{coupl} .

The coupling capacitor C_{coupl} protects the signal processor **110** inputs from the transmit signal voltage. The signal processor **110** includes the internal clamping diodes **D2** which provide the current to charge the coupling capacitor to the transmit voltage. Thus, the coupling capacitor takes up nearly all of the transmit voltage, while the diodes **D2** hold the voltage present at the signal processor **110** input at plus or minus one diode drop (e.g., 0.7 V).

Because the coaxial cables **122** mainly are used for both transmit and receive, the transmit waveform would also appear (without the transmit blocking circuitry) at the signal processor **110** output. The capacitor C_2 and diodes **D4** protect the signal processor **110** output from the transmit voltage. Specially, **D4** clamps the signal to one diode drop while C_2 decouples the signal processor **110** output from the transmit waveform by taking up the majority of the transmit voltage.

The transmit waveform is sufficiently filtered by the coaxial cable **122** to limit the charge current for the capacitors C_2 and C_{coupl} .

During receive, the receive signals from the transducer elements **E** pass through C_{coupl} to the signal processor **110**. The signal processor **110** input stage is a charge amplifier **A** with gain determined by C_{coupl} . In general, for a good noise figure, the impedance of the coupling capacitor should be small compared to the impedance of the transducer element **E**. However, a small impedance value increases the charge current during transmit.

Because the voltage on the transducer element is small during receive, the diodes **D1** are open. The diodes **D1** thus operate as a low voltage signal blocker to decouple the transducer elements **E** from each other. The echo signals received from the transducer elements are delayed and summed inside the signal processor **110** and provided to the receive section output **710**. More specifically, the output signal passes through the output resistor **R** and the capacitors **C1** and **C2** to the coaxial cable **122**. The load from the host system **116** preamplifier and the coaxial cable **122** capacitance is large enough to limit the output voltage at **D4** to be less than the diode on-voltage. Thus, the diodes **D4** are open-circuit during receive.

The resistor **R** effectively controls the signal gain into the coaxial cable **122**. The value of the protection capacitor **C2** (similar to the input coupling capacitor) is a trade-off between transmit surge current and receive impedance. In one implementation, the capacitor **C2** is approximately 100 pF. The capacitor **C1** decouples the output DC level from the clamping diodes **D4**. The precise value for **C1** is not critical, but may be set to be several times the value of **C2** (e.g., 1 nF) in order to avoid signal reduction due to **C1**.

The shunt capacitor C_{shunt} reduces the crosstalk from the receive section output **710** back to the receive section input **712**. More specifically, even though the diodes **D3** are in the off state during receive, their parasitic capacitance in the pF range will create crosstalk. The shunt capacitor is large compared to the parasitic capacitance and presents a much lower impedance than the parasitic capacitance. As a result, the diode **D3** and shunt capacitor create a voltage divider where the majority of the voltage drops off at the parasitic capacitance, while the shunt capacitor takes only a small voltage drop. Thus, the small voltage on the shunt capacitor effectively limits cross talk. Note that during transmit, when the diodes are essentially short-circuits, the shunt capacitor is a negligible load compared to the coaxial cable **122** capacitance.

FIG. 8 shows the bottom layer **802** and top layer **804** side of a processing board **106**. FIG. 8 shows an exemplary layout plan for the processing electronics included on each processing board **106** as described in detail above with regard to FIG. 7. As shown in FIG. 8, the signal processors **110** may occupy the central area of the processing boards, while the **D1** diode arrays may be located below the signal processor **110** and the **D3** and **D4** diode arrays may be located above the signal processors **110**.

Turning next to FIG. 9, that figure shows a block diagram **900** of a signal processor **110**. The signal processor **110** includes four aperture processors **902**, **904**, **906**, and **908**, a digital control block **910**, and support circuitry that may include a delay tuning circuit **912**, a recovery voltage circuit **914**, and a bias circuit **916**.

Each aperture processor **902-908** includes sixteen receive inputs (e.g., s0In0-s0In15) that are connected to transducer elements that form a receive sub-aperture. In one embodiment, the receive sub-aperture is triangular and formed from

fifteen transducer elements. Thus, one input on each sub-aperture processor **902-908** may go unused. Each sub-aperture processor **902-908** also includes a test input (labeled **testin**) and digital control inputs (labeled **pgm**). The sub-aperture processors **902-908** perform beamforming on the receive input signals and output the beamformed signal obtained over the receive sub-aperture on the receive sub-aperture outputs (labeled **s0Out-s3Out**).

The digital control block **910** includes clock (**sClk**, e.g., a 20 MHz system clock), data (**sDataIn0** and **1**, serial data inputs and **sCdataIn**, a serial control data input), and control (**sOEN**, an output enable for the signal processor **110**) signals. The digital control block also includes two data outputs (**sDataOut0** and **1**). The data inputs and outputs may be used to chain signal processors **110** in series as noted below.

The circuitry in the signal processor **110** is described in more detail below with regard to FIG. **10**. FIG. **10** shows the narrowband beamforming circuitry in the signal processor **110**. Each receive input (one of which is labeled **sxIn0**) passes through a low-noise amplifier **1002**, a weighting and summation stage including mixers (one of which is labeled **1004**), summers (a positive summation summer labeled **1005** and a negative summation summer labeled **1006**), and all-pass filters **1008** and **1009**. In addition the all-pass filters connect to second summers (one of which is labeled **1010**) and through a line driver **1012** out to the receive sub-aperture output (one of which is labeled **sxOut**).

The low-noise amplifiers (LNA) are charge sensitive amplifiers that amplify the receive signal from a transducer element via the external coupling capacitor. The LNA gain may be set by adjusting the ratio between the external coupling capacitor and an internal feedback resistor. Typically the open loop gain for the LNA is high, while typical closed loop gain (at 3 MHz) is selected to exploit the available signal range.

The LNAs have fast recovery time in part due to the recovery voltage circuit **914**. If the receive signal voltage drive the circuitry into saturation recovery circuitry is activated to ensure fast recovery from the input stage saturation.

As shown in FIG. **10**, Inphase (I) and Quadrature (Q) signals are generated from the receive signals. To that end, each input is given weight and sign depending on the desired channel delay before all the inputs are summed. A multi-input amplifier does the weighting and summing by employing individually selectable input capacitor sizes on each input. A fully differential amplifier may be employed for the summation. The sign of each input is set by feeding the input either to the positive summation node **1005** or negative summation node **1006**.

In one embodiment, the signal processor **110** uses the following weights shown in Table 2 and Table 3 for 22.5 degree quantization.

TABLE 2

Phase	IMx	qMx
$0 \leq \text{phase} < \pi/2$	1	1
$\pi/2 \leq \text{phase} < \pi$	-1	1
$\pi \leq \text{phase} < 3\pi/2$	-1	-1
$3\pi/2 \leq \text{phase} < 2\pi$	1	-1

TABLE 3

Phase	In	qn
0	1	0
$\pi/8$	0.924	0.383
$\pi/4$	0.707	0.707
$3\pi/8$	0.383	0.924
$\pi/2$	0	1
X	0	0

The summation stage **1010**, having the second summers, may further include an attenuation to level the signal swing of the available range.

The all-pass filters impart, to the I and Q signals, phase delays chosen to minimize differential phase error over a frequency band of interest. Each filter has a first-order transfer function given in the s-plane by $H(s) = (1-st)/(1+st)$, where t is the RC time constant of the filter. The transfer function may be realized using resistors and cross-coupled capacitors with active feedback. More specifically, the all-pass filters may be implemented as a non-inverting buffer followed by a resistor, in parallel with an inverting buffer in series with a capacitor (See FIG. **20**).

In one embodiment, the all-pass filter **1008** has $RC=25$ ns, and the all-pass filter **1009** has $RC=145$ ns at 3 MHz. The determination of **iMx**, **qMx**, **in**, and **qn** are described below with regard to FIG. **15** and Table 4.

The line driver **1012** drives the beamformed receive signal back to the host system **116**. The line driver **1012** may use a opamp with a very large output stage connected as a combination of a summer and difference amplifier. In this fashion, the signal from the I and Q channels are summed and converted into a single ended output. The gain of the combined second summation stage and line driver are selected to give the desired output range.

The delay tuning circuitry **912** is included to account for variations in process and operating conditions that may alter the time constants of the allpass filters. To control the time constants, the tuning circuit **912** is included.

The bias circuit **916** controls the bias currents to the analog modules in the signal processor **110**. The power supply voltage may be used as a reference voltage. In one implementation, the bias current is distributed over the signal processor **110** to supply the different analog modules with the required bias current.

Turning next to FIG. **13**, that figure shows a block diagram of the digital interface **1300** of the signal processor **110** that is included in the digital control block **910**. The digital interface **1300** includes four pairs of six-bit registers/memories **1302** and **1304**, **1306** and **1308**, **1310** and **1312**, and **1314** and **1316** for storing delta Y and delta X inclination parameters for the four receive apertures handled by the signal processor **110**. The digital interface **1300** also includes two 1-bit bank memories **1318**, **1320**, two data shift registers **1322**, **1324**, a multi-bit key register **1326**, and a multi-bit command register **1328**. The tri-state buffers **1330** and **1332** allow the interface **1300** to place its outputs in a high impedance state under control of the **SOEN** signal.

The interface **1300** may be used to program, set up and read from the signal processor **110**. The interface **1300** includes a command line (**SCDATAIN**), two data lines (**SDATAIN0**, **1**), one enable line (**SOEN**), and one clock line **SCLK** (not shown). The **SDATAIN0** and **SDATAIN1** lines provide for serial data input to the two data shift registers **1322**, **1324** (labeled **SHIFTREGISTER0**, **1**), while **SCDATAIN** provides for serial data input to a control data shift register. In one

implementation, the data shift registers may be 25 bits long, while the control shift register may be 36 bits long.

The signal processor **110** is typically used in a hostile environment where the digital input lines are expected to assume random values during ultrasound-transmission. To avoid getting false data and commands through the digital interface, the 32 bit key register is used as an enable signal. When the correct key resides in the key register (compared to the key pre-selected and pre-set in the signal processor **110**), the digital controller executes the command placed in the 4 bit command register.

The data lines may be shifted simultaneously into the registers controlled by the SCLK data clock. SCLK runs, for example, at 20 MHz. Note that the interface **1300** also includes two digital outputs labeled SDATAOUT0 and SDATAOUT1. These outputs are the outputs of the data shift registers and may be used to connect multiple signal processors **110** in a chain (See FIG. 14). Output data from the signal processors **110** are shifted through the serial chain and read out from the last signal processor **110** in the chain.

Because the output-bus is connected to the input-bus in the chain, the SOEN signal may be employed to place the output of the last signal processor **110** in tristate mode (Hi Z mode) when writing to the chain. When reading out data over the serial bus, SOEN may be used to enable the output from the last signal processor **110**.

In one implementation, the 36-bit control data register includes of a 32-bit key register and a 4-bit command register. The SCDATAIN line may be a separate signal line to all signal processors **110** on a processor board **106**. In addition, as shown in FIG. 13, the serial shift registers are shifted in from most significant bit (MSB). In other words, command and data is shift in LSB first.

Also shown in FIG. 13 are the six bit inclination parameter memories that store location information for the four receive sub-apertures handled by the signal processor **110**. The pair of six-bit memories **1302**, **1304** store delta Y and delta X inclination information for a receive sub-aperture and the pair of six-bit memories **1306**, **1308** store delta Y and delta X inclination parameters for a second receive sub-aperture. Similarly, the pair of six-bit memories **1310**, **1312** store delta Y and delta X inclination parameters for a third receive sub-aperture and the pair of six-bit memories **1314**, **1316** store delta Y and delta X inclination parameters for a fourth receive aperture. Then loading the signal processor static information (geometry ram, setup registers, encoder ram, etc.) the shift register division is adapted to the data loaded.

Turning briefly to FIG. 14, that figure shows a serial chain **1400** of signal processors **110**. The serial chain **1400** is connected through the SDATAOUT0, SDATAOUT1, SDATAIN0, and SDATAIN1 signal lines. A clock line, latch line, and parameter selection line (for selecting which parameter registers to write) may also be provided.

Turning next to FIG. 15, that figure shows a cross-point controller **1500** in the signal processor **110** that calculates new control values for processing the four receive sub-apertures assigned to the signal processor **110** based on the delta X, delta Y inclinations loaded through the serial interface (See FIG. 13). The cross-point controller **1500** will calculate 16 new delay settings for each aperture, based on new inclinations parameters delta X, delta Y. The delay setup are calculated based on the contents of the geometry RAM and the new inclinations parameters delta X, delta Y. The corresponding phase delays are found from lookup in the chosen encoder RAM bank.

To that end, the cross-point controller **1500** includes the multipliers **1502**, **1504**, and a summer **1505**. The cross-point

controller **1500** also includes a controller **1506**, a geometry ram **1508**, and an encoder ram **1510**. Four sets (one for each receive sub-aperture) of sixteen 5-bit phase setting registers **1512**, **1514**, **1516**, and **1518** are provided (a total of 64 five-bit registers). These delay setting registers store the delay setting control bits for each receive sub-aperture handled by the signal processor **110**, as noted below.

The geometry RAM **1508** holds the relation between a receive signal channel n , and the corresponding transducer location (x_n, y_n) within the receive sub-aperture. The encoder RAM **1510** holds the relation between the coded delay and the hardware settings $(iM_{xn}, in, qM_{xn}, qn)$ shown in FIG. 10 for narrowband beamforming. Alternatively, the encoder RAM **1510** holds the relation between the desired delay and the cross-point switch control signals $intPol$, $chPos(4)$, and $sign$ for the broadband beamforming circuitry shown in FIG. 19. The parameter δX_n represents the x-inclination for sub-aperture n , $n=0, 1, 2, 3$, while δY_n represents the y-inclination for sub-aperture n , $n=0, 1, 2, 3$ for each of four sub-apertures handled by the processor **110**.

When a valid key is detected in the key register and the start cross-point calculation command is selected, the cross-point controller **1500** calculates new register values for sub-apertures **0**, **1**, **2** and **3**. Because up to 16 receive signals may contribute to each receive aperture, a total of 64 calculations are performed. The delta X and delta Y values shown in FIG. 15 are the values loaded from the serial interface prior to each new setup. All eight delta X and delta Y values loaded during the previous setup calculation are available to the cross-point controller **1500** via two 24 bit buses as shown in FIG. 13.

To save setup time, the data to be used in the next calculation is shifted in and loaded while the signal processor is calculating the current setup. When the current calculation is finished, the new delta X and delta Y data have been loaded and are ready for the next setup calculation.

To start a calculation the key and command register are loaded with the key value and the bit code assigned to the desired command. When a calculation is initiated, delta X and delta Y values for aperture **0** are put on the multiplier **1502**, **1504** inputs. A sequencer **1506** controls the calculations. The sequencer **1506** may be implemented as an up counter that cycles through all 64 receive signal inputs (4 sub-apertures times 16 receive inputs per sub-aperture). The sequencer **1506** is connected to the address bus of the geometry RAM **1508**. The data for one sub-aperture is generally calculated before advancing to the next sub-aperture.

The sequencer **1506** also controls routing the signal from the encoder RAM **1510** to the correct analog sub-aperture register **1302-1314**, as well as the multiplexing of the correct delta X and delta Y data to the cross-point controller **1500**. In one implementation for narrowband beamforming, the output from the Encoder RAM **1510** is a 5 bit word, called $sap_data[4:0]$ that maps to $sX_m_controlX()$.

$sX_m_controlX()$ maps to the control signals for the beamforming circuitry shown in FIG. 10. The five bits $sX_m_control4.0(Y)$ directly control the angular weight and sign to the Y channel (receive signal) for aperture X. The translation from bit values to angular weight and sign is given in Table 4. In other words, the Encoder RAM **1510**, for narrowband beamforming, maps from a delay value to the multiplexer sign $(iM_{xn}$ and $qM_{xn})$ and the I and Q scaling $(in$ and $qn)$. These parameters implement 16 phase angles, and to be able to omit signals with given delays, $in=qn=0$ may also be selected. As a result, the word length in the Encoder RAM **1510** is 5 bits. Alternatively, the bits in the Encoder RAM **1510** may directly choose coefficients and multiplexer values

(e.g., using one bit for each multiplexer, and 3 bits with decoder to select each of the six gain-pairs in Table 3).

The encoder RAM **1510** has a 10 bit address bus and a 5 bit data bus. To start loading data to encoder RAM **1510**, the

TABLE 4

Mapping between SAP control bits and phase										
#	bit4	bit3	bit2	bit1	bit0	iMxn	in	qMxn	qn	Phase
0	0	0	0	0	0	1	1.0	X	0.0	0
1	0	0	0	0	1	1	0.924	1	0.383	Pi/8
2	0	0	0	1	0	1	0.707	1	0.707	Pi/4
3	0	0	0	1	1	1	0.383	1	0.924	3Pi/8
4	0	0	1	0	0	X	0.0	1	1.0	Pi/2
5	0	0	1	0	1	-1	0.383	1	0.924	5Pi/8
6	0	0	1	1	0	-1	0.707	1	0.707	3i/4
7	0	0	1	1	1	-1	0.924	1	0.383	7Pi/8
8	0	1	0	0	0	-1	1.0	X	0.0	Pi
9	0	1	0	0	1	-1	0.924	-1	0.383	9Pi/8
10	0	1	0	1	0	-1	0.707	-1	0.707	5Pi/4
11	0	1	0	1	1	-1	0.383	-1	0.924	11Pi/8
12	0	1	1	0	0	X	0.0	-1	1.0	3Pi/2
13	0	1	1	0	1	1	0.383	-1	0.924	13Pi/8
14	0	1	1	1	0	1	0.707	-1	0.707	7Pi/4
15	0	1	1	1	1	1	0.924	-1	0.383	15Pi/8
16...31	1	X	X	X	X	X	0.0	X	0.0	X

The calculations may be done with 2's complement number representation. Referring again to FIG. **15**, the delta X and delta Y and geometry RAM data are multiplied and summed in the summer **1505**. This calculation produces a 13 bit output. Because delta X and delta Y are never maximal at the same time, in the calculations the two MSBs will always be the same and the MSB of the signal can be truncated. In the implementation shown in FIG. **15**, precision is reduced to 8 bits truncating the four LSBs.

The cross-point controller **1500** sequences through all transducer element receive inputs 'n' for every receive aperture 'm' handled by the signal processor **110**. The cross-point controller **1500** may be considered to determine a scaled version of the delay to be introduced to each receive signal as: $\text{floor}((x(m,n)*\text{deltaX}(m)+y(m,n)*\text{deltaY}(m))/16)$, for $n=0, 1, \dots, 15$, and $m=0, 1, 2, 3$.

Note that $x(m,n)$ and $y(m,n)$ are the geometrical positions of the transducer element coupled to the nth input for receive aperture m. The positions are indexed through the geometry RAM **1508** to add routing flexibility during processing circuit board **106** layout. The inclination parameters $\text{deltaX}(m)$ and $\text{deltay}(m)$ may remain constant for all receive signals in a given receive sub-aperture m, but may typically vary between the sub-apertures.

The calculated delay is converted into a physical delay through a table look-up in the encoder RAM **1510**.

With regard to the geometry RAM **1508**, it takes a 6 bit address and stores 12 bit data. To start loading data to the geometry RAM **1508**, the command RESET_ADDR_COUNTERS is issued to reset the address counters. The next command is then LOAD_GEOM_RAM, which will write data to the current addresses pointed to by the address counter, and auto-increment the address counter. Because the datawidth is 12 bit, one shift/load procedure will load 4 datawords into the geometry RAM **1508**. The address counter will therefore be incremented by 4 at each load.

The encoder RAM **1510** is divided into four banks, reflecting four different frequency settings for the ultrasound probe **100**. The bank0 and bank1 registers loaded from the serial interface specify which bank is used. Together with the eight bits from the calculation, they make up the encoder RAM address in the 1024x5 bit RAM.

command RESET_ADDR_COUNTERS is issued to reset the address counters. The next command is LOAD_ENC_RAM, which will write data to the current addresses pointed to by the address counter and bank 0/1 registers, and auto-increment the address counter. Since the data width is 5 bit, one shift/load procedure will load 8 aperture control data words to the RAM **1510**. The address counter will therefore be incremented by 8 at each load.

Bits [19:0] in both serial shift registers are used for data to the RAMs. Bit **24** of serial shift register **0** is mapped to the bank 0 control signal for the encoder RAM **1510**, and bit **24** of serial shift register **1** is mapped to the bank 1 control signal. Bank 0/1 registers (See FIG. **13**) control which bank is loaded. In one embodiment, the location memory controller **112** sends four-bit commands to the signal processors **110**. The commands are shifted into the signal processors **110** into the command register **1328**. Exemplary commands are presented below in Table 5:

TABLE 5

Name	Command
RESET	Places the signal processor into a known state
LOAD_X_Y_Data	Load delta X and delta Y and encoder bank from shift register.
RESET_ADDR_COUNTERS	Reset all address counters for reading and writing to the signal processor.
LOAD_GEOM_RAM	Load 4 datawords to geometry RAM.
LOAD_ENC_RAM	Load 8 datawords to encoder RAM.
CALCULATE	Calculate new aperture beamforming values.
DELAY_TUNING_START	Start analog tuning and calibration procedure.
WRITE_ANALOG_MP_REG	Write to the analog multi-purpose register in the signal processor.
READ_ANALOG_MP_REG	Put the analog multi-purpose register, containing, for example, the delay measurement from the delay tuning, on the 1322, 1324.
READBACK_REGS	Read out the internal registers of the signal processor.
WRITE_REGS	Write directly to the internal registers of the signal processor.
LOAD_PD_REG	Write a analog power-down register.

FIG. 16 summarizes the steps 1600 that the ultrasound probe 100 shown in FIG. 1 may take to perform sub-aperture processing. The probe 100 receives, at signal processors 110 distributed over processing boards 106, multiple receive signals from acoustic transducer elements (Step 1602). The transducer elements may form triangular receive sub-apertures that are wholly processed by a given signal processor 110, rather than being partitioned between processing boards. During the receive (and transmit) operations, the probe 100 multiplexes at least one of the acoustic transducer elements between the receive sub-aperture and a square transmit sub-aperture (Step 1604).

After beamforming, the signal processor 110 drives a receive sub-aperture output with a beamformed signal obtained over the acoustic transducer elements in the receive sub-aperture (Step 1606). In the transmit direction, the probe may couple transmit signals to multiple transmit sub-apertures over transmit signal connections distributed between multiple processing boards (Step 1608). Like the receive apertures, the transmit signal connections for a given sub-aperture may all be provided on a given processing board 106, rather than being partitioned across multiple processing boards 106.

Not partitioning the transmit or receive sub-apertures between multiple processing boards provides for efficient routing of signals between the host system 116 and the processing boards 106 to the transducer array 102. Because each processing board 106 processes its own transmit and receive sub-apertures, no cross-connecting signals or routing needs to be provided between the processing boards 106.

FIG. 17 summarizes the steps 1700 that the ultrasound probe 100 shown in FIG. 1 may take to perform beamforming in the probe 100. The probe 100 receives multiple directional parameters such as inclination values (e.g., delta X and delta Y data) for the receive sub-apertures from a host system 116 at a cache memory and controller 112 (Step 1702). The cache memory and controller 112 then transfers the directional parameters to multiple signal processors 110 on multiple processing boards 106 (Step 1704).

The probe 100 couples to signal processors 110, receive signals arising from a receive sub-aperture (Step 1706). The signal processor 110 retrieves, from the serial input registers (e.g., 1302-1304, 1306-1308, 1310-1312, or 1314-1316), directional parameters for the receive sub-aperture (Step 1708). Based on the directional parameters, the signal processor determines a beamforming delay for the transducer elements in the receive sub-aperture (Step 1710), and applies the delay to the receive signal from each respective transducer element (Step 1712).

FIG. 18 shows steps 1800 that the ultrasound probe 100 shown in FIG. 1 (e.g., using the transceiver circuitry 700 may take to transmit and receive energy to an acoustic transducer element multiplexed between a receive aperture and a transmit aperture.) The circuitry 700 couples a transmit pulse through a transmit section input 704, a transmit section output 706, and receive signal blocking circuitry D1, D3 and Cshunt coupled between the transmit section input 704 and the transmit section output 706 (Step 1802). The transceiver circuitry 700 also couples a receive signal through a receive section input 712, a receive section output 710, and transmit signal blocking circuitry C2 and D4, and Ccouple and D2, coupled between the receive section input 712 and the receive section output 710 (Step 1804).

Turning next to FIG. 19, that figure shows a block diagram 1900 of another implementation of beamforming circuitry in the aperture processors 902-908. The beamforming circuitry 1900 includes the pre-amplifiers 1902, one for each of sixteen

receive channels in a receive aperture, and one for testing. The pre-amplifiers 1902 are connected to a 34x11 cross-point matrix 1904 that flexibly connects the receive signals through zero to ten delay elements 1906 and summing nodes 1908 that form, in series, a delay line. The line driver 1910 drives the combined signal back to the host system 116.

The cross-point matrix 1904 supports the connection of any receive channel to any node of the delay line. When several channels are connected to the same node of the delay line, then the output of that node is the sum of the respective input signals. Any channel may be inverted before entering a summing node, and any channel may optionally be simultaneously connected to two adjacent summing nodes. In that case, the signal will then split so that the effective gain is reduced by approximately 6 dB for each.

When the beamforming circuitry 1900 is employed, the cross-point controller 1500 outputs the following signals to the beamforming circuitry 1900: intPol, chPos(4).

FIG. 11 shows one implementation for an all-pass filter cell (e.g., the filter cell 1906). As shown, the all-pass filters may be implemented as a non-inverting buffer followed by a resistor R, in parallel with an inverting buffer in series with a capacitor C. Each filter cell has a phase delay of $T=2RC$, and a transfer function of $H_c(w)=(1-j(wT/2))/(1+j(wT/2))$.

FIG. 12 shows a cross-point controller 2100 for use with the beamforming circuitry 1900 to program the switches in the cross-point matrix 1904, starting on a trigger event and operating on the latched version of the scan parameters. The cross-point controller 2100 sequences through all transducer element receive inputs 'n' for every receive aperture 'm' handled by the signal processor 110. The cross-point controller 2100 may be considered to determine a preliminary scaled version of the delay to be introduced to each receive signal as: $\text{floor}((x(m,n)*\text{deltaX}(m)+y(m,n)*\text{deltaY}(m))/8)$, for $n=0, 1, \dots, 15$, and $m=0, 1, 2, 3$.

Note that $x(m,n)$ and $y(m,n)$ are the geometrical positions of the transducer element coupled to the nth input for receive aperture m. A reserved code may be established (e.g., $x(m,n), y(m,n)=-16, -16$) that disables (e.g., for power management) channel n of the aperture m by using the decoder 2102 to detect the code (or optionally or in addition, overflow of chPos), and assert a channel disable output signal. The positions are indexed through the geometry RAM 1508 to add routing flexibility during processing circuit board 106 layout. The scale factors $\text{deltaX}(m)$ and $\text{deltay}(m)$ may remain constant for all receive signals in a given receive aperture m.

The preliminary delay is converted into a physical delay through a table look-up in the encoder RAM 1510. In one implementation, the output of the encoder RAM 1510 includes six bits: one bit for intPol, four bits for chPos, and one bit for sing. The chPos bits cause the corresponding switch in the cross-point matrix 1904 to be closed. If the control bit intPol is set, the switch 1+chPos will also be set. The sign bit selects the non-inverted or inverted version of the input signal.

While various embodiments of the invention have been described, it will be apparent to those of ordinary skill in the art that many more embodiments and implementations are possible that are within the scope of this invention.

What is claimed is:

1. A sub-aperture beamforming probe including an array of transducer elements, the probe comprising:
 - a handheld ultrasound probe housing;
 - a first processing board comprising a first signal processor located in the probe housing;
 - a plurality of transducer elements held in the probe housing and coupled to receive signal connections of the first

signal processor to define a receive sub-aperture, the receive signal connections coupling receive signals arising from the transducer elements to the first signal processor; and

a cache memory in the probe housing and coupled to the first signal processor, the cache memory comprising directional parameters associated with receive beams for the receive sub-aperture;

where the first signal processor retrieves directional parameters associated with one of the receive beams, determines a beamforming delay derived from the directional parameters for each transducer element in the receive sub-aperture, and applies the respective beamforming delay to each receive signal.

2. The beamforming probe of claim 1, where one of the directional parameters is an inclination value.

3. The beamforming probe of claim 1, wherein the beamforming delay is implemented as a phase shift.

4. The beamforming probe of claim 1, wherein the cache memory comprises static setup information including at least one of locations of the transducer elements defining the receive sub-aperture and delay setting mapping tables associated with the transducer elements defining the receive sub-aperture.

5. The beamforming probe of claim 1, wherein the directional parameters stored in the cache memory comprises dynamic setup information containing directional information for the receive sub-aperture that varies from beam to beam.

6. The beamforming probe of claim 1, where:

the first signal processor retrieves the directional parameters for first and second receive sub-apertures, determines a beamforming delay derived from the directional parameters for each transducer element in first and second receive sub-apertures, and applies the beamforming delays to the receive signals obtained from the respective transducer element.

7. The beamforming probe of claim 1, further comprising a cache memory controller located in the probe housing and coupled to the cache memory, the cache memory controller incrementing an address pointer through pages in the cache memory to read out select pages the directional parameters.

8. The beamforming probe of claim 7, further comprising a communication interface coupled to the cache memory controller for interfacing with a system host.

9. The beamforming probe of claim 8, where the cache memory controller obtains the directional parameters using the communication interface.

10. The beamforming probe of claim 1, further comprising: a second processing board comprising a second signal processor located in the probe housing;

a plurality of second transducer elements held in the probe housing and coupled to second receive signal connections of the second signal processor to define a second receive sub-aperture, the second receive connections coupling second receive signals arising from the second transducer elements to the second signal processor; and the cache memory coupled to the second signal processor, the cache memory comprising second directional parameters associated with receive beams for the second receive sub-aperture;

where the second signal processor retrieves the second directional parameters associated with one of the receive beams for the second receive sub-aperture, determines a beamforming delay derived from the second directional parameters for each transducer element in the second

receive sub-aperture, and applies the respective beamforming delay to each second receive signal.

11. The beamforming probe of claim 1, wherein the plurality of transducer elements are arranged spatially in a triangular pattern.

12. The beamforming probe of claim 1, wherein the plurality of transducer elements have adjacent rows of elements constituting part of the receive sub-aperture with different first and second numbers of elements in the adjacent rows.

13. The beamforming probe of claim 1, wherein the cache memory stores directional set up information for all receive beams in a receive scan sequence associated with the receive sub-aperture.

14. The beamforming probe of claim 1, wherein the cache memory stores directional information divided into pages, where each of the pages contains directional information associated with a different receive beam of a receive beam of a receive scan sequence.

15. A sub-aperture beamforming probe comprising:

a handheld ultrasound probe housing;

a first processing board comprising a first signal processor located in the probe housing;

a second processing board comprising a second signal processor located in the probe housing; and

a plurality of transducer elements held in the probe housing and coupled to the first and second signal processors to define a plurality of receive sub-apertures;

where the transducer elements associated with each receive sub-aperture are coupled to at least one of the first and second signal processors without partitioning any receive sub-aperture between the first and second processors; and

a cache memory located in the probe housing and coupled to the first signal processor, the cache memory comprising directional parameters for a selected receive sub-aperture coupled to the first signal processor.

16. The beamforming probe of claim 15, where the first signal processor:

retrieves the directional parameters for the selected receive sub-aperture; and

determines, for a selected transducer element of the selected receive aperture, a beamforming delay derived from the directional parameters.

17. The beamforming probe of claim 15, where the first signal processor applies the beamforming delay to a receive signal arising from the selected transducer element on a beam by beam basis.

18. The beamforming probe of claim 15, wherein the cache memory is coupled to the second signal processor, the cache memory comprising beam dependent directional parameters for a selected receive sub-aperture coupled to the second signal processor.

19. The beamforming probe of claim 15, where the transducer elements associated with at least one of the receive sub-apertures are spatially arranged in a triangular pattern.

20. The beamforming probe of claim 15, further comprising a receive sub-aperture output driven by the first signal processor to carry a sub-aperture beamformed receive signal for the selected receive sub-aperture.

21. The beamforming probe of claim 15, further comprising a location memory coupled to the first signal processor, the location memory comprising a spatial location for a selected receive sub-aperture.

22. The beamforming probe of claim 15, wherein at least a portion of the receive sub-apertures comprise different first and second numbers of transducer elements arranged in at least first and second adjacent rows of transducer elements.

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23. The beamforming probe of claim 15, wherein the cache memory stores the directional parameters divided into pages, the first signal processor reading one of the pages of the directional parameters at a time in connection with corresponding receive signals.

24. A method for performing sub-aperture beamforming in an ultrasound probe where the probe includes a handheld probe housing that holds a plurality of transducer elements, a first signal processor and cache memory, the method comprising:

coupling, to the first signal processor, receive signals arising from the transducer elements associated with a receive sub-aperture;

retrieving, from the cache memory, a beam related directional parameter for the receive sub-aperture; and

determining a beamforming delay derived from the directional parameter for a selected transducer element associated with the receive sub-aperture.

25. The method of claim 24, further comprising applying the beamforming delay, within the probe housing, to a receive signal arising from the selected transducer element.

26. The method of claim 24, further comprising applying a plurality of beamforming delays to a plurality of receive signals from the transducer elements associated with the receive sub-aperture.

27. The method of claim 24, where coupling comprises coupling receive signals from the transducer elements associated with a plurality of receive sub-apertures to the first signal processor on a first processor board in the probe housing and to a second signal processor on a second processor

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board in the probe housing; where no receive sub-aperture is partitioned between the first and second processing boards.

28. The method of claim 24, further comprising storing a spatial location in a location memory located in the probe housing.

29. The method of claim 24, further comprising receiving the directional parameter from a host system over a system cable.

30. The method of claim 24, further comprising maintaining a link between the cache memory and a host system according to a standard defined by IEEE 1596.

31. The method of claim 24, further comprising:

receiving a plurality of directional parameters for receive sub-apertures coupled to the first processor and a second processors from a host system at a cache memory controller; and

transferring the directional parameters for receive sub-apertures coupled to the first processor to the first processor board and transferring the directional parameters for receive sub-apertures coupled to the second processor to the second processor board.

32. The method of claim 24, further comprising inputting to the first signal processor a test signal configured to do at least one of calibrate and verify operation of the first signal processor.

33. The method of claim 24, further comprising storing, in memory on the probe, a key containing information validating probe commands.

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