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(54) **ULTRASOUND PROBE TRANSCEIVER CIRCUITRY**

Publication Classification

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(57) **ABSTRACT**

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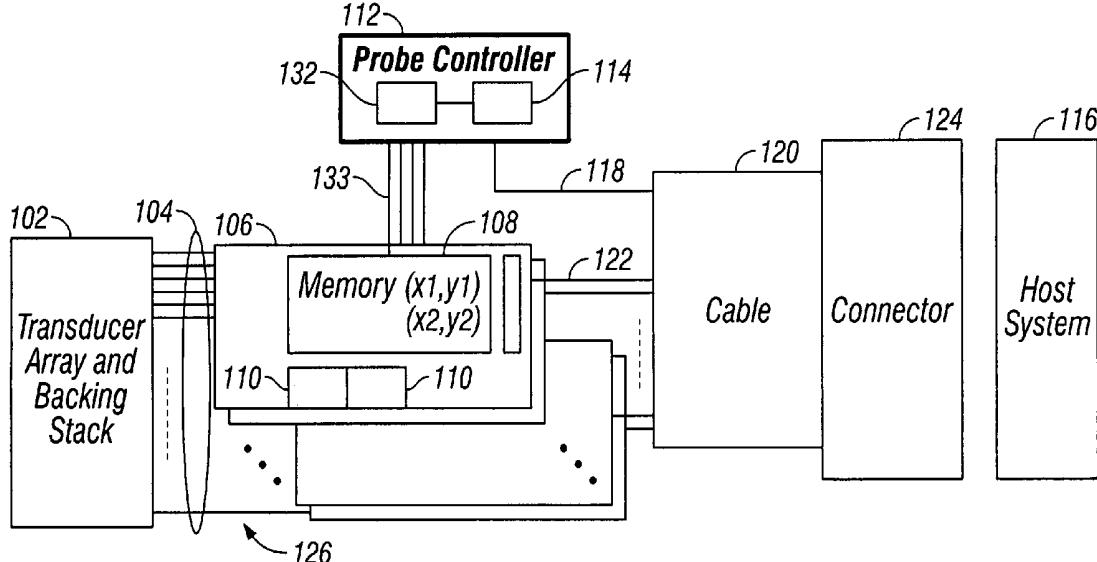
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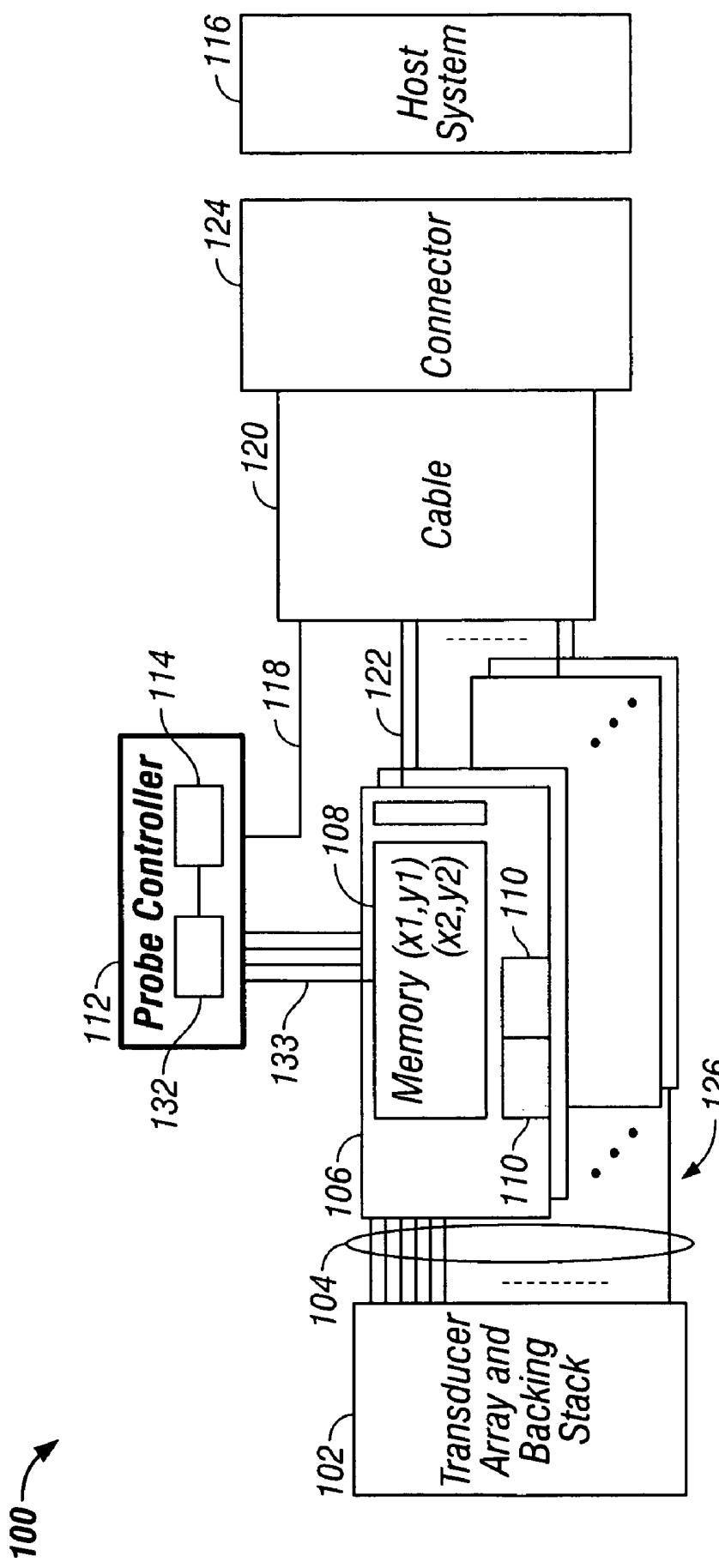
(21) Appl. No.: **10/719,431**

(22) Filed: **Nov. 21, 2003**

Transceiver circuitry for ultrasound transducer elements includes a transmit section and a receive section. The transmit section includes a transmit section input, a transmit section output, and receive signal blocking circuitry connected between the transmit section input and the transmit section output. The receive section includes a receive section input, a receive section output, and transmit signal blocking circuitry connected between the receive section input and the receive section output.

100



**FIG. 1**

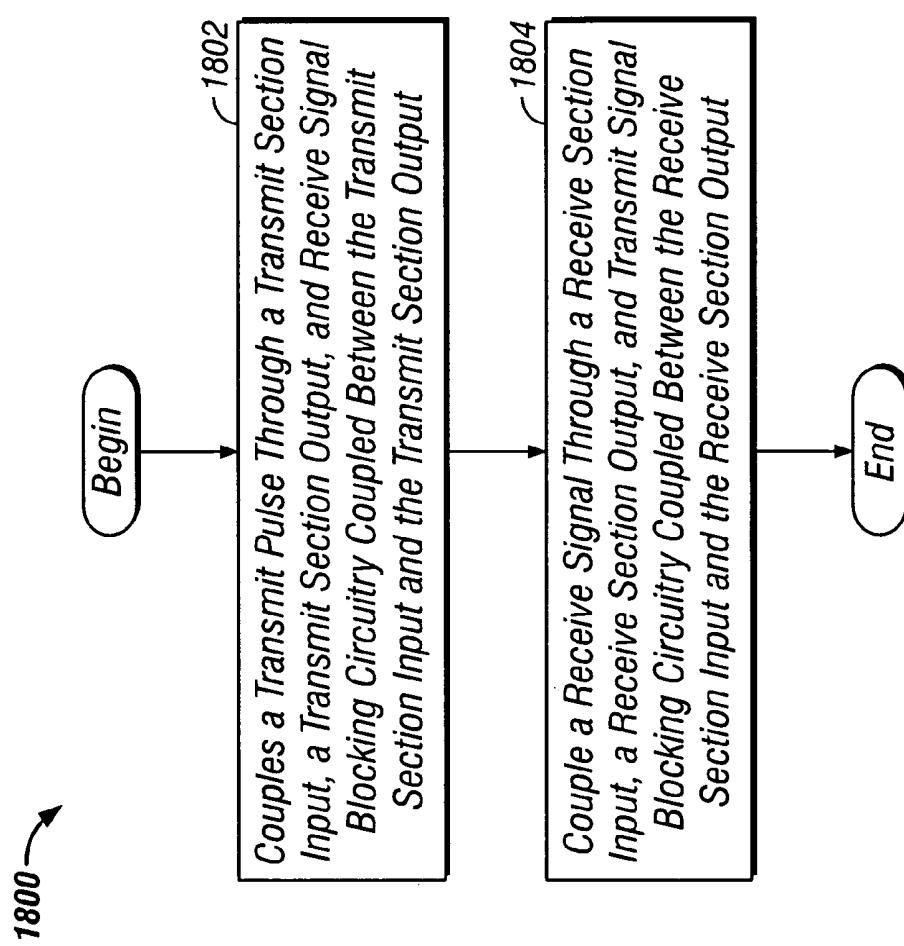


FIG. 18

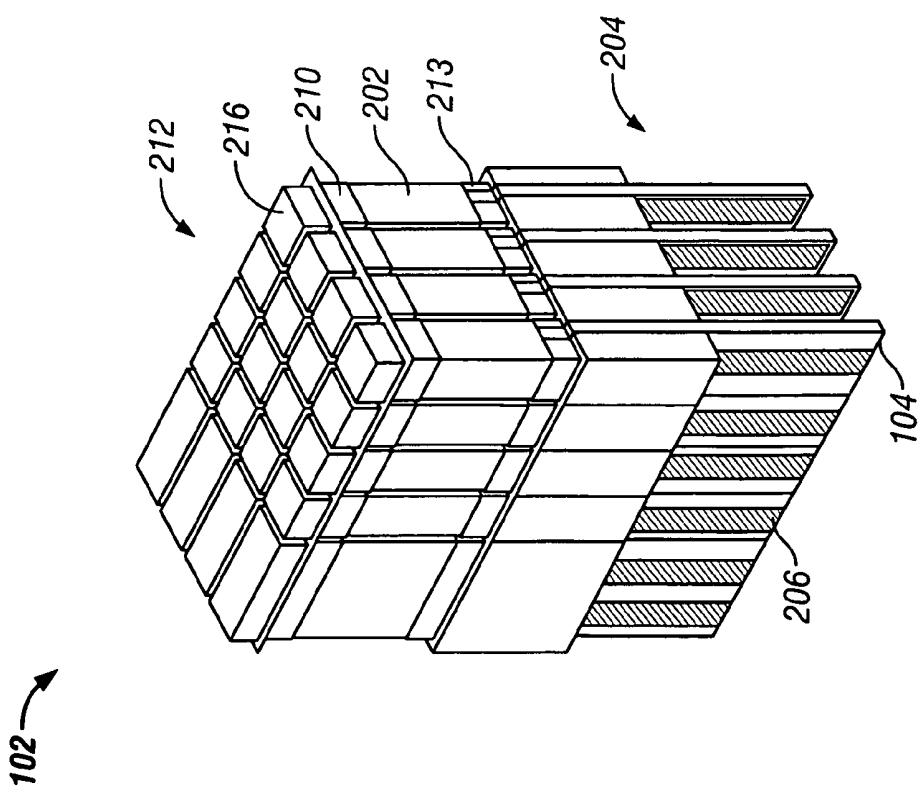


FIG. 2

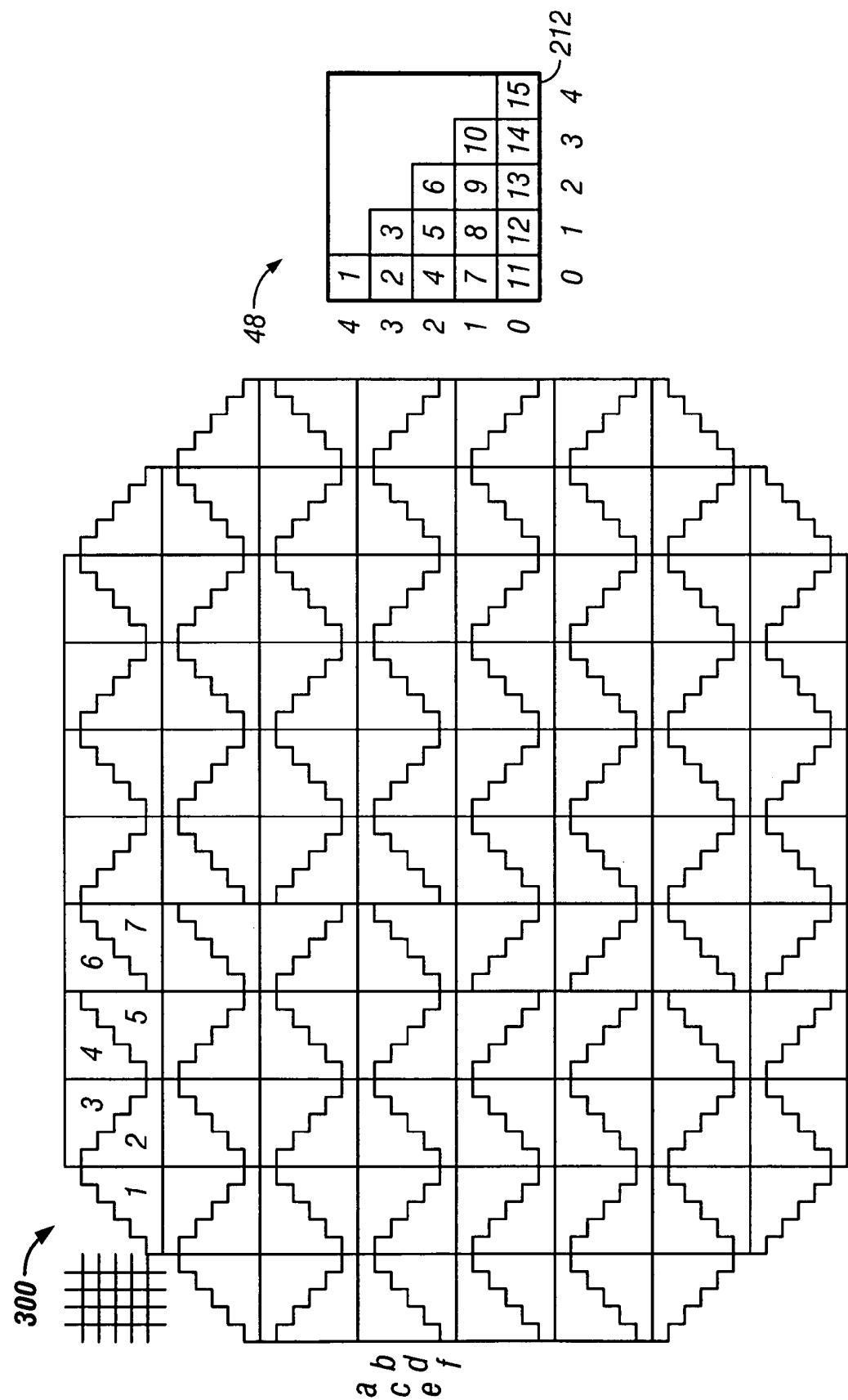


FIG. 3

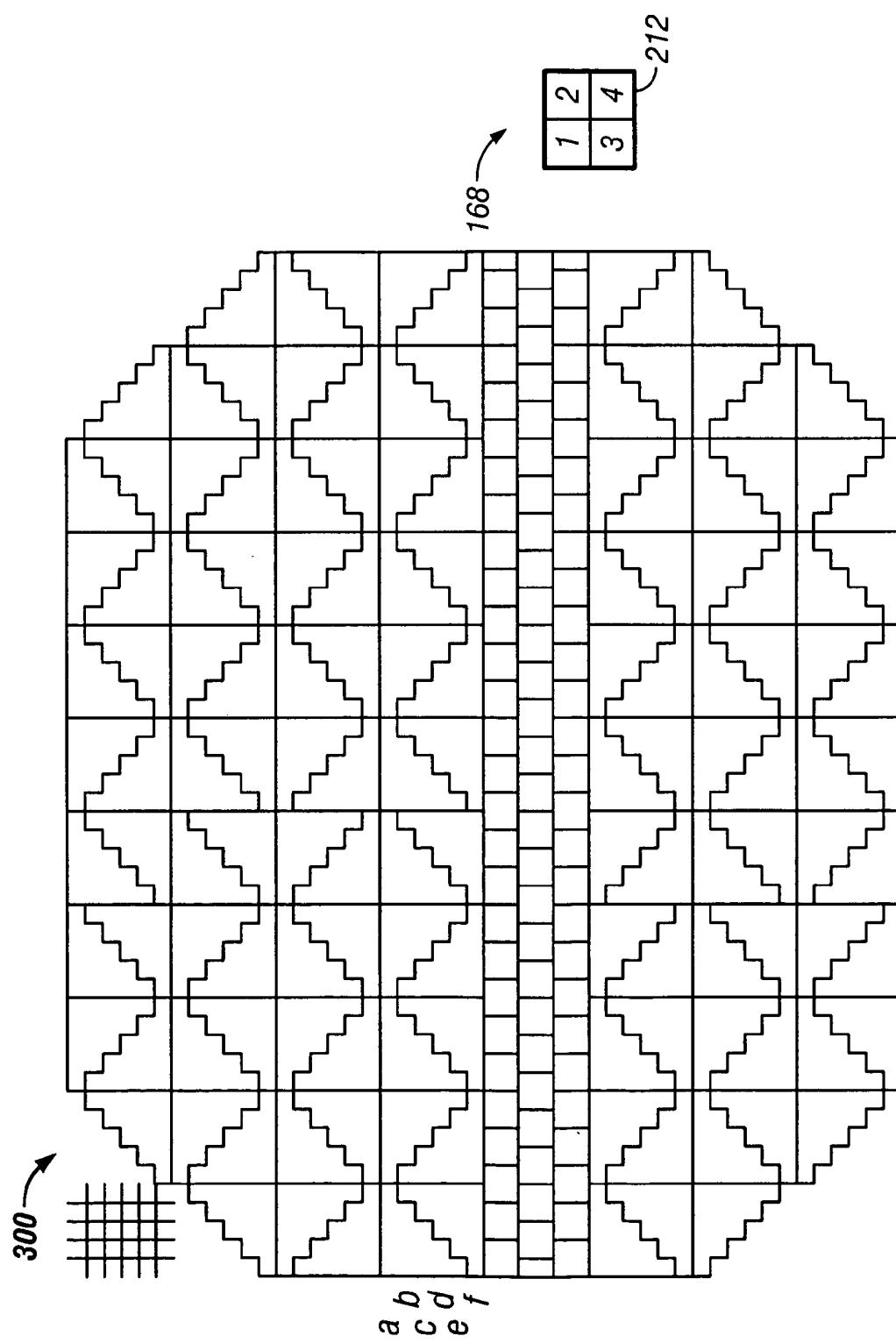


FIG. 4

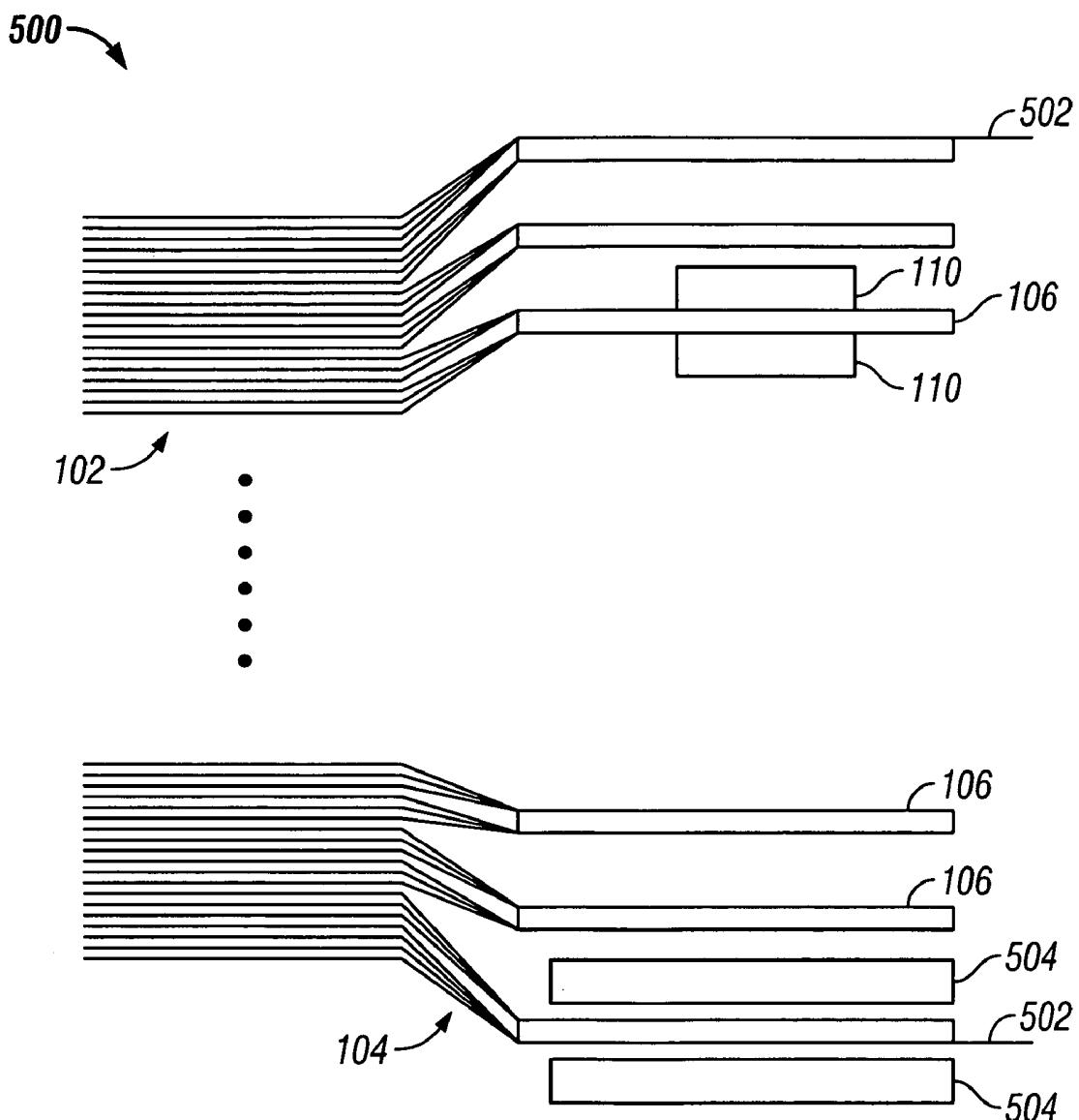


FIG. 5

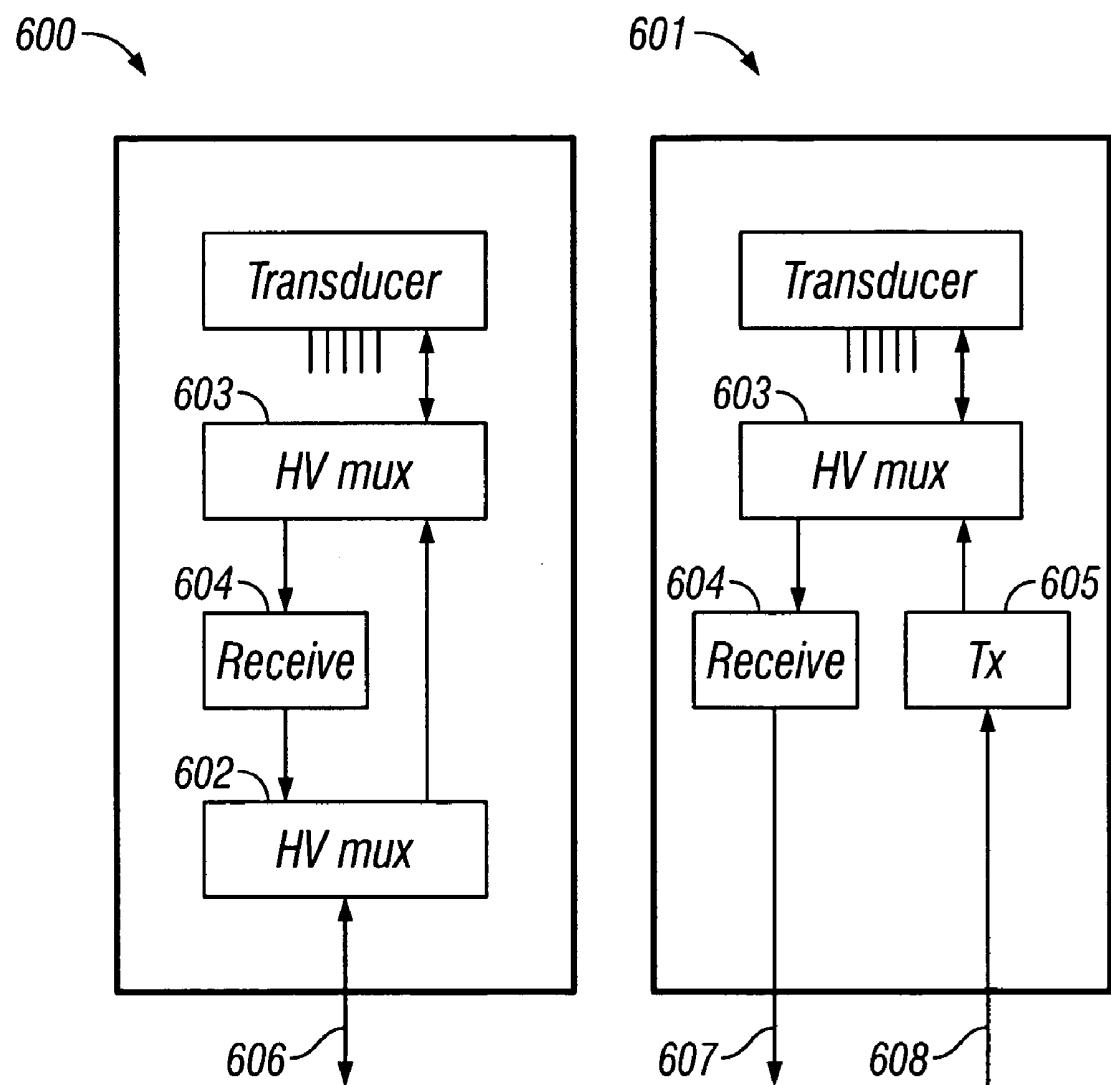
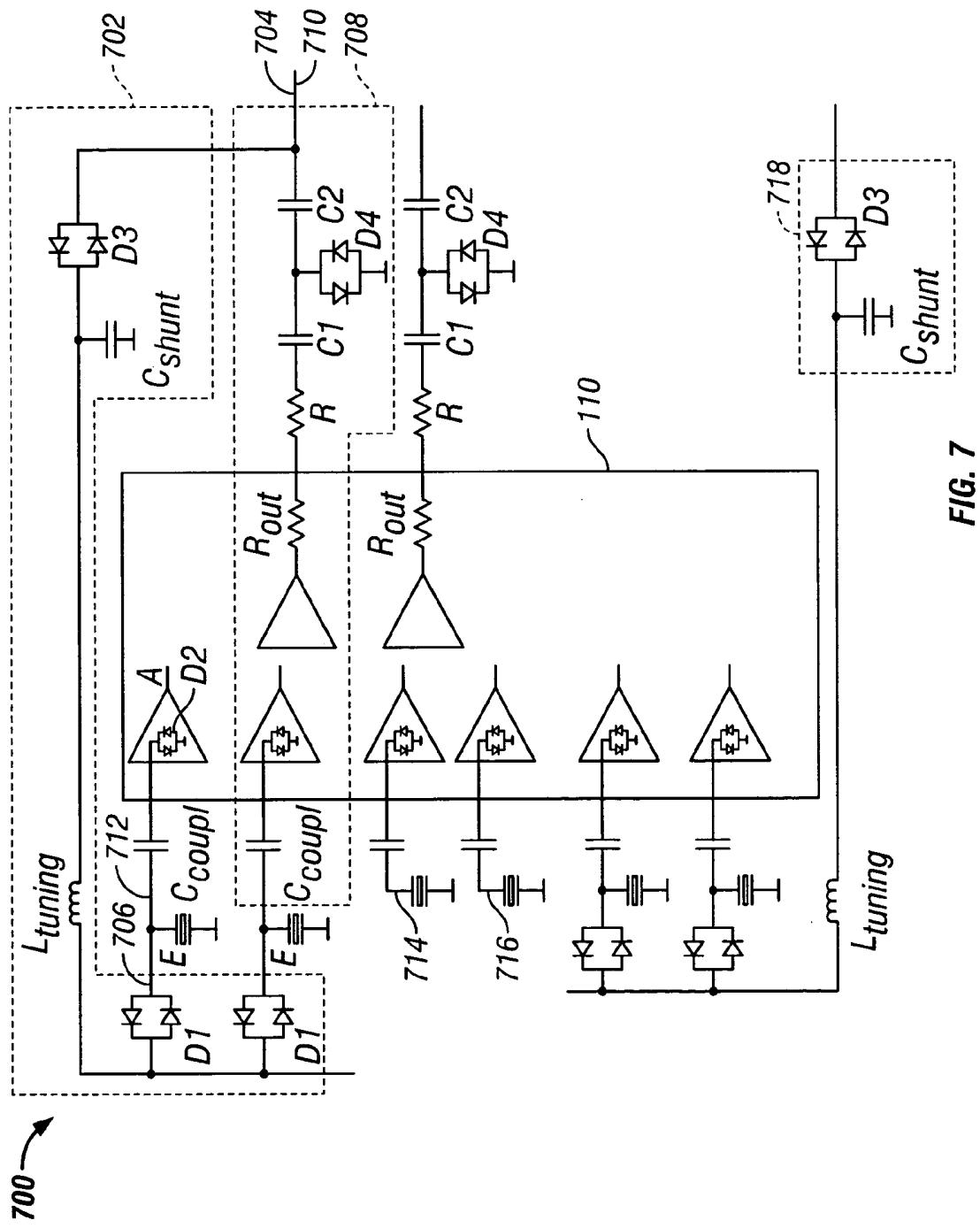
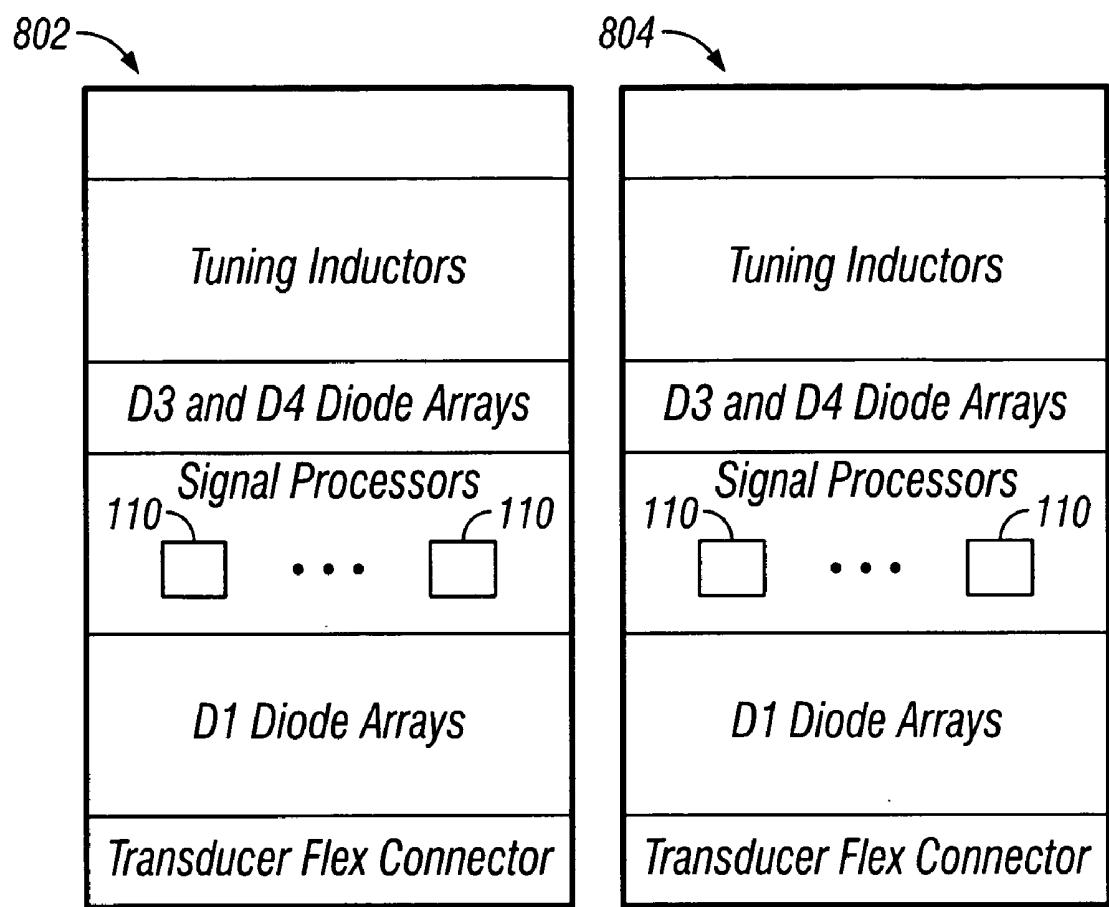
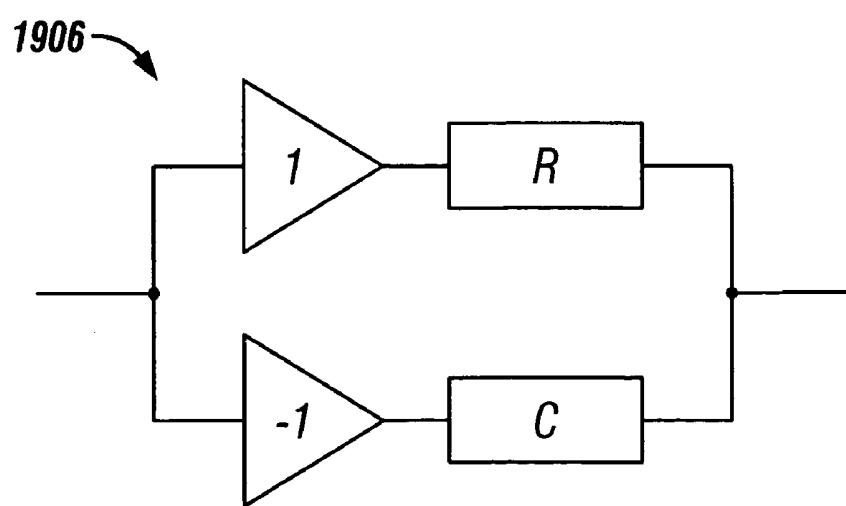


FIG. 6



**FIG. 8****FIG. 11**

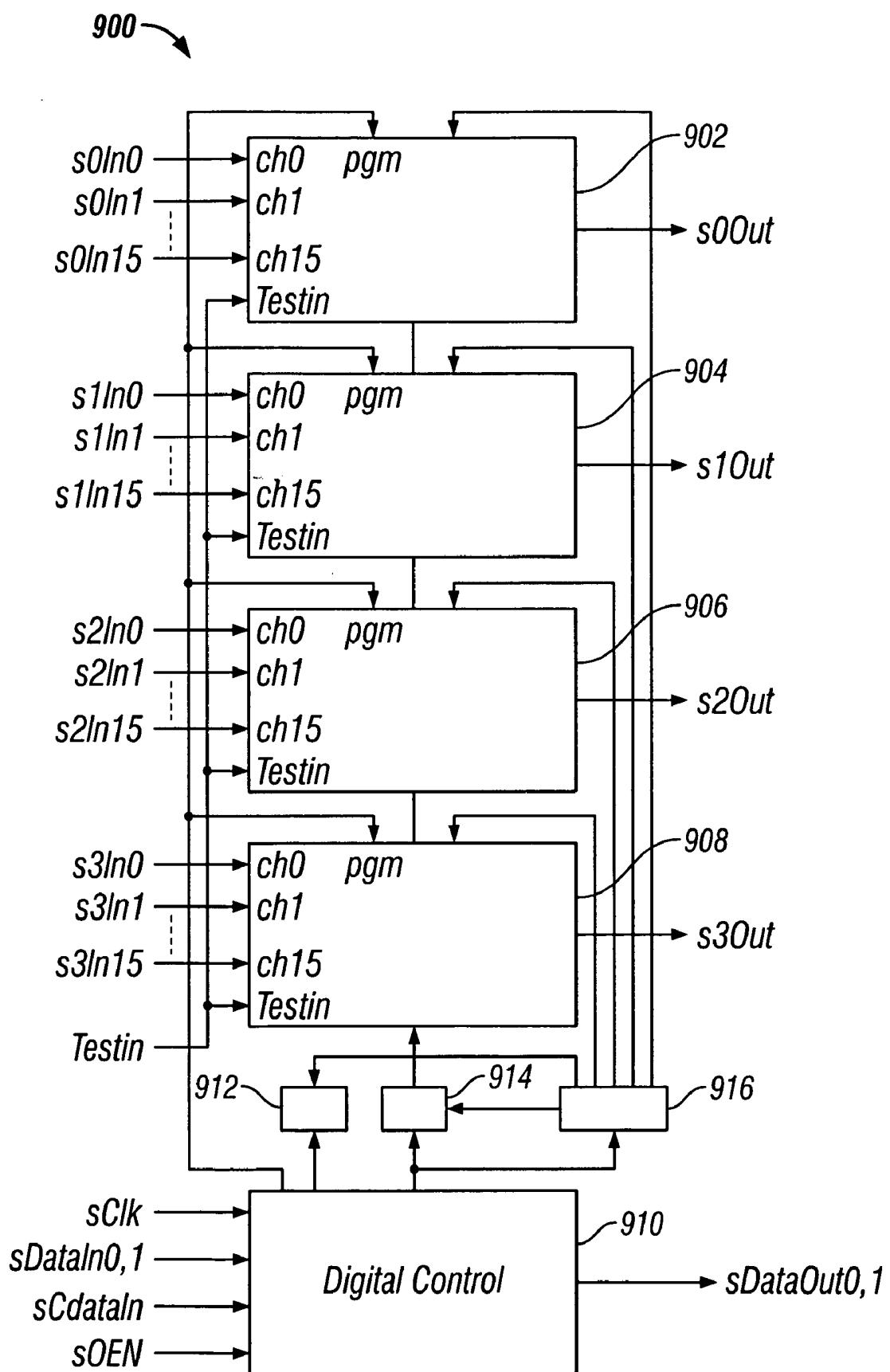


FIG. 9

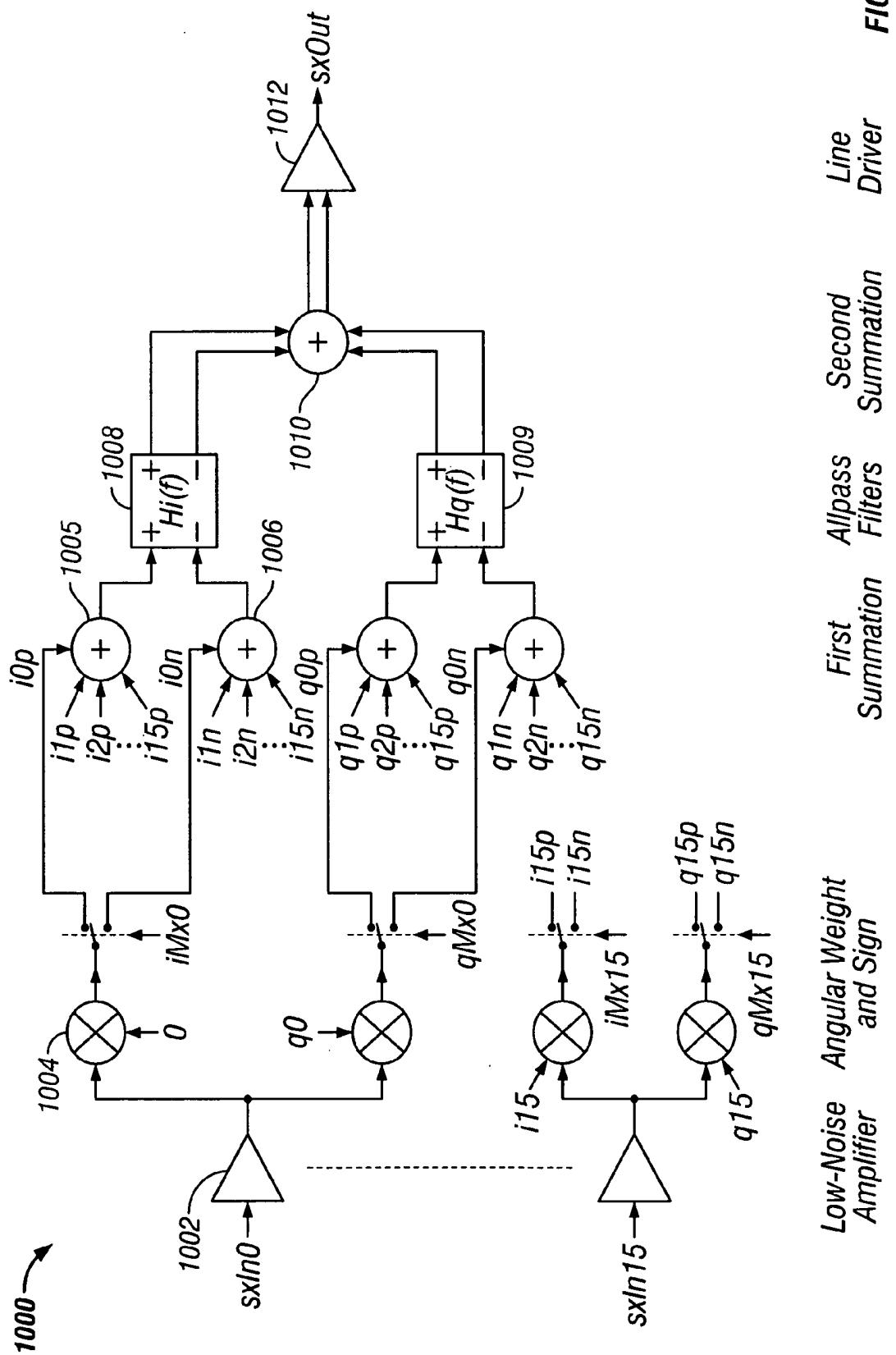


FIG. 10

 Line
Driver

 First
Summation
Allpass
Filters
Second
Summation

 Low-Noise
Amplifier
Angular Weight
and Sign

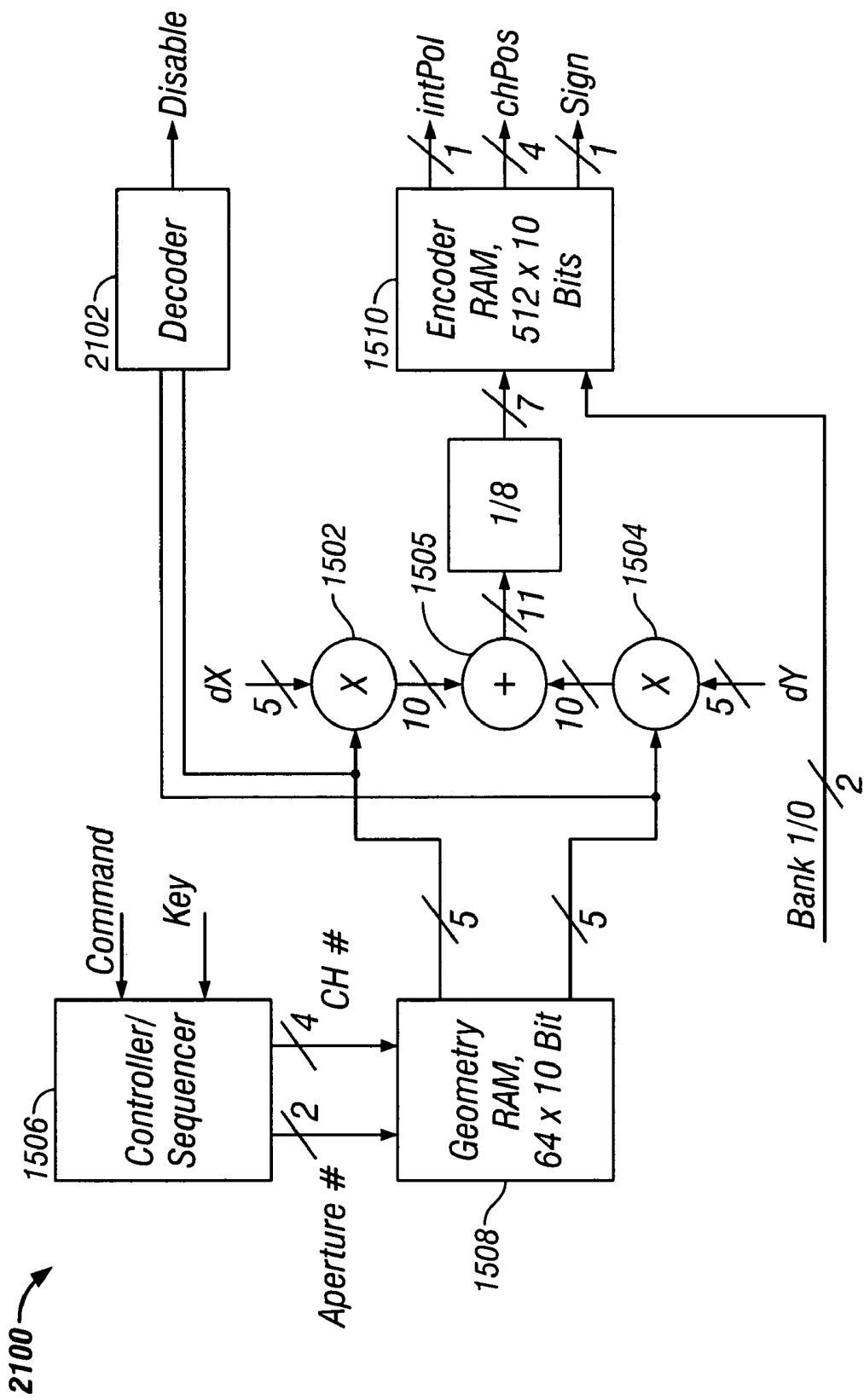


FIG. 12

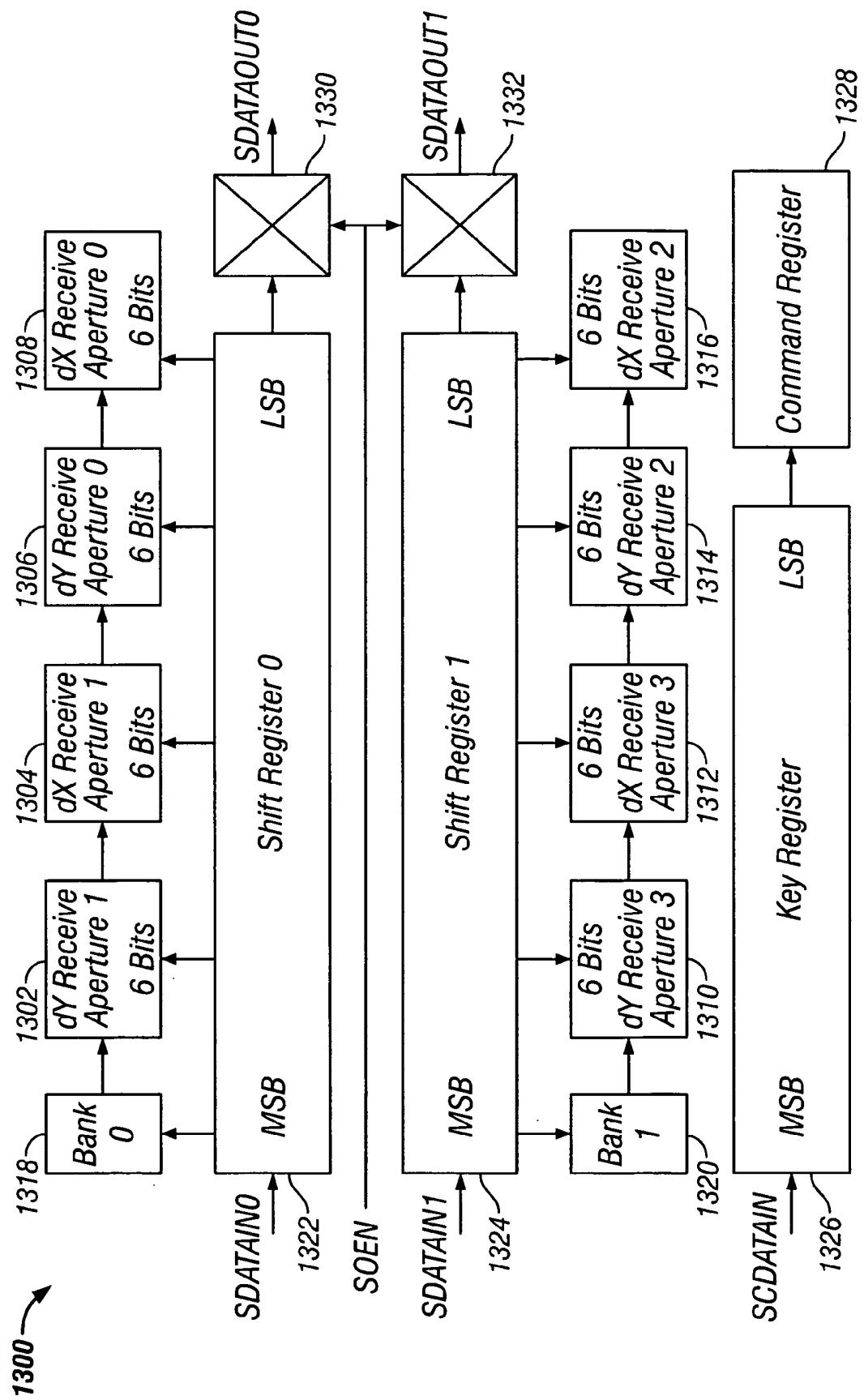


FIG. 13

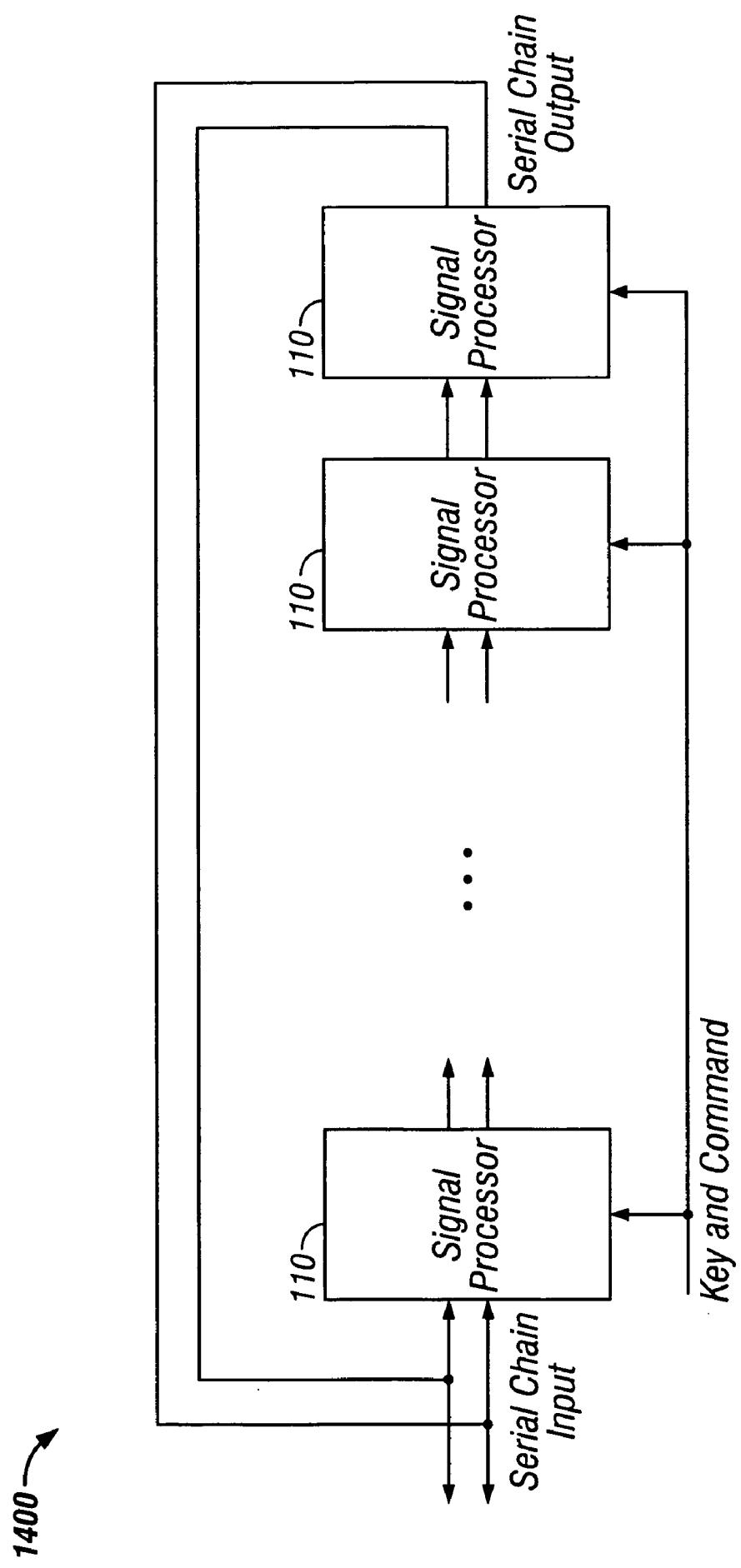


FIG. 14

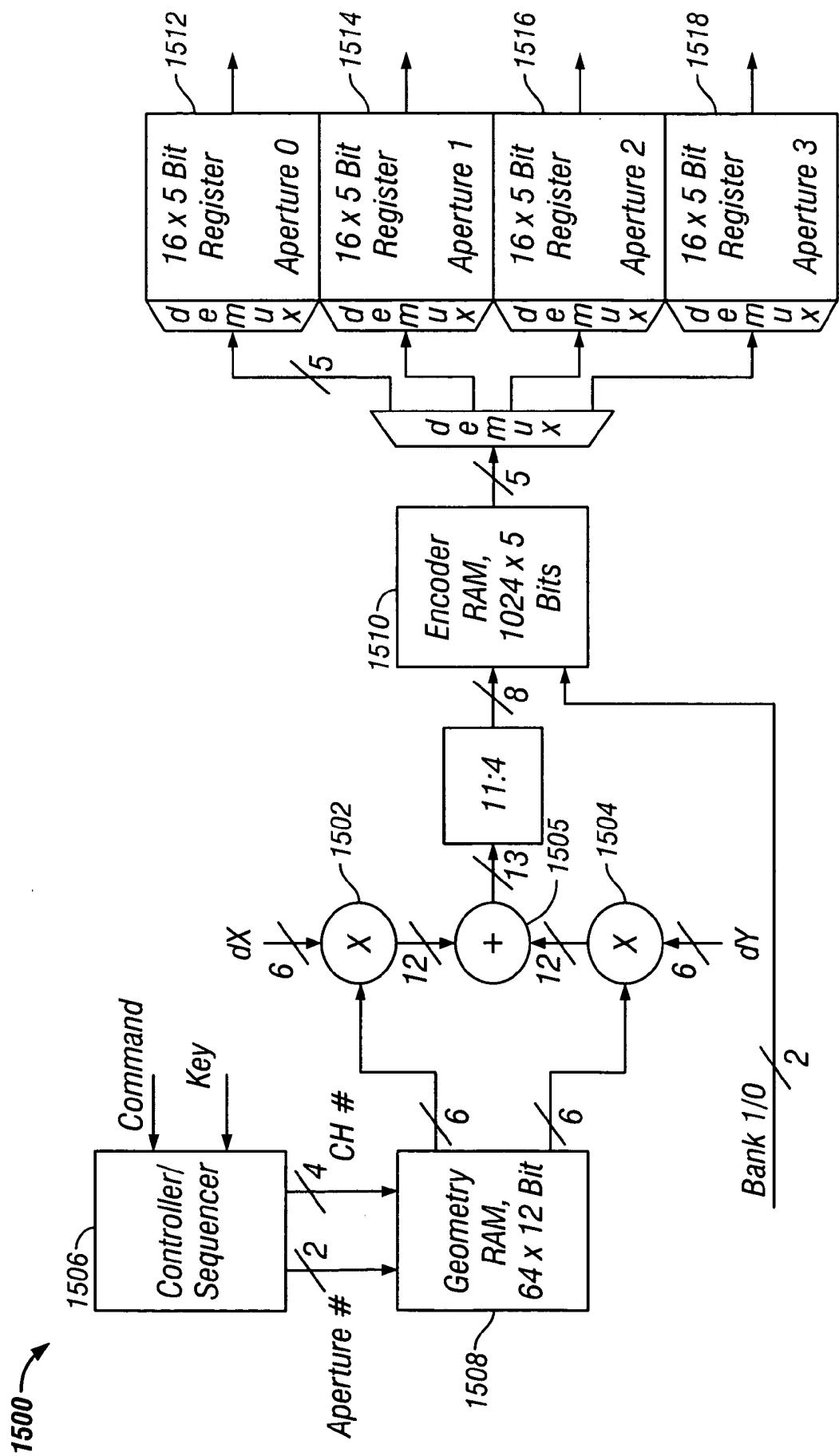


FIG. 15

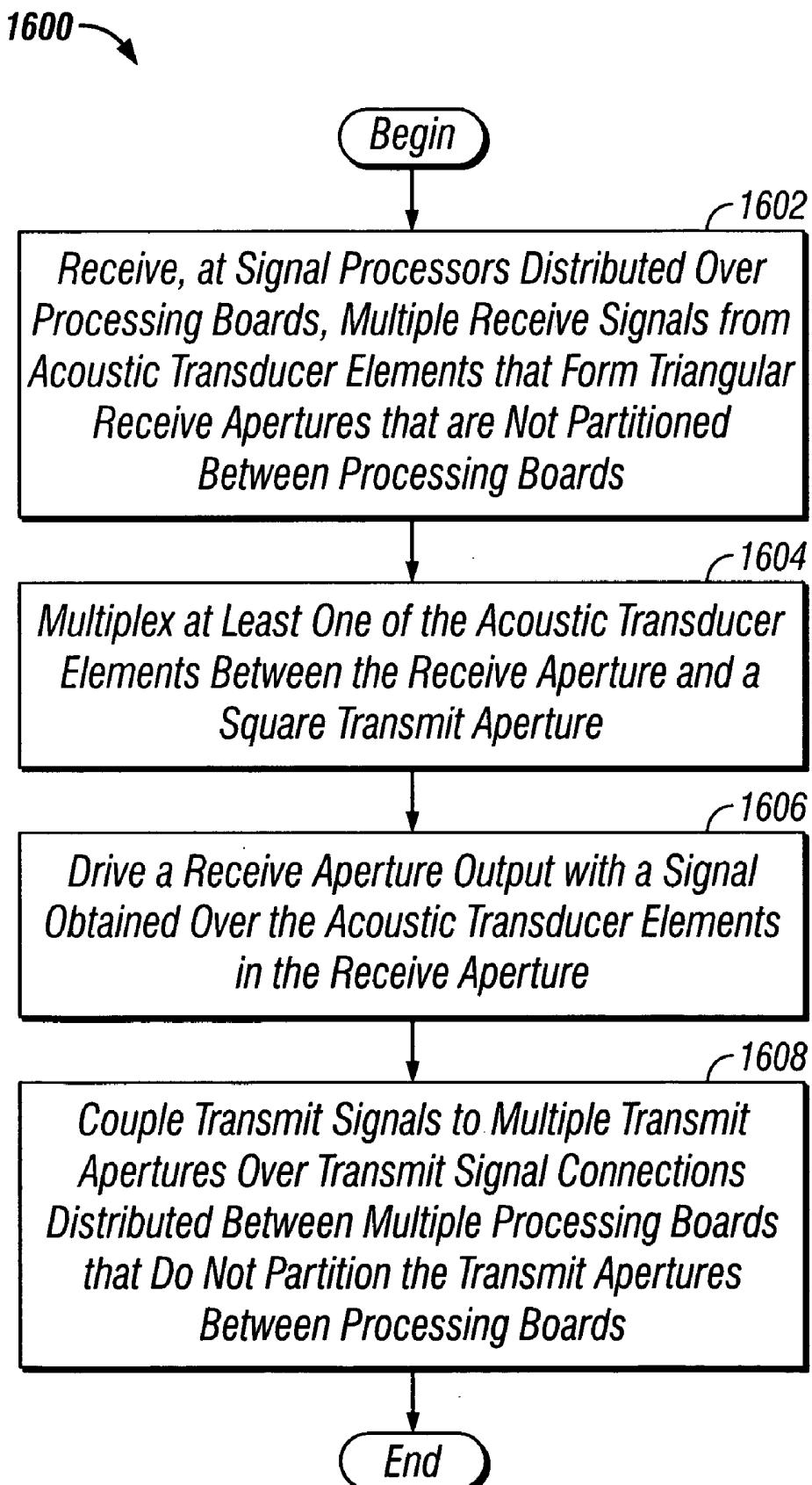


FIG. 16

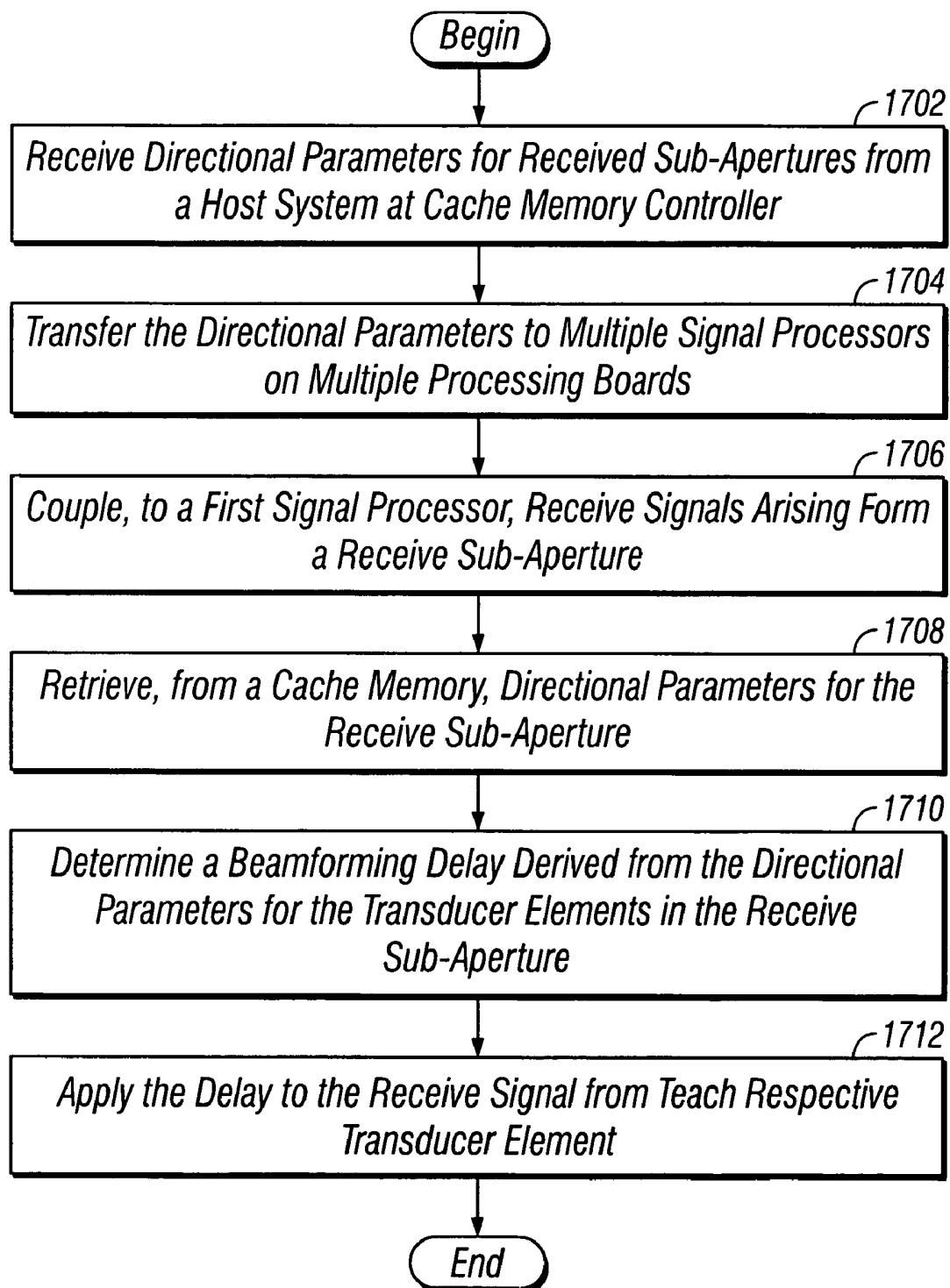
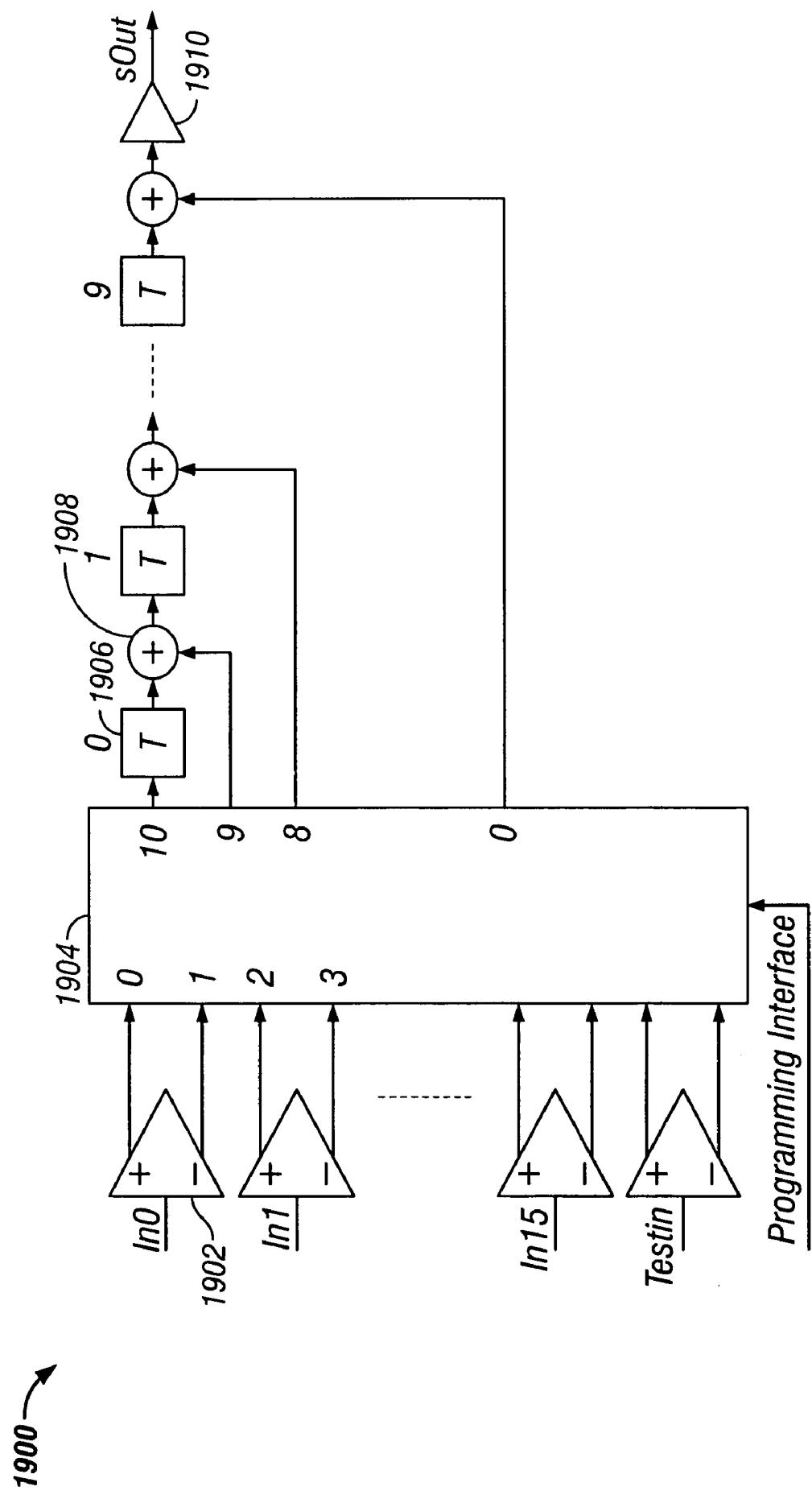


FIG. 17



ULTRASOUND PROBE TRANSCEIVER CIRCUITRY

CROSS REFERENCE TO RELATED APPLICATIONS

[0001] This application is related to Docket No. 135274, Titled "Ultrasound Probe Distributed Beamformer", filed Nov. 21, 2003, Ser. No. _____, and Docket No. 135271, Titled "Ultrasound Probe Sub-Aperture Processing", filed Nov. 21, 2003, Ser. No. _____.

BACKGROUND OF THE INVENTION

[0002] 1. Field of the Invention

[0003] This invention relates generally to ultrasound medical imaging systems. More specifically, this invention relates to processing sub-apertures of a multiple element transducer probe.

[0004] 2. Related Art

[0005] Doctors and technicians commonly use medical imaging systems to obtain display, and study images for diagnostic purposes. In ultrasound imaging systems, for example, a doctor may obtain images of a patient's heart in an attempt to learn whether the heart functions properly. As time moves forward, these imaging systems become increasingly adept at obtaining not only the images but also additional related diagnostic information such as ECG traces, heart rate, and the like.

[0006] Two key components of an ultrasound system are the ultrasound probe and the beamformer. The beamformer focuses and steers ultrasound energy transmitted by and received by the probe as one step in generating images of anatomic content on a display.

[0007] Development of 3D ultrasound push towards ultrasound probes with a large number of acoustic elements. Recent technology developments suggest reducing the large number of channels by sub-grouping the aperture elements and preprocess each group into one signal that is transferred to the system. Transmit can similarly be handled by transmitters solely in the probe, or by transmitting on sub-groups of the aperture.

[0008] High quality images, of course, are of great importance in clinically evaluating the physiology that a doctor is studying. High quality images require use of a non-sparse aperture, e.g. most elements on the aperture must be used both for transmit and receive. Current system, achieve this by multiplexing between the transmit and receive circuitry in the system. Each channel in the probe can then be connected with one cable to the system and be used both for transmit and receive.

[0009] The layout and implementation of the aperture sub-grouping for transmit and receive is of great importance for the image quality. The introduction of circuitry in the probe poses technical challenges that must be solved. Also, with receive and/or transmit circuitry in the probe the current approach with a transmit/receive switch in the system does not allow use off all acoustic channels on the probe for both transmit and receive.

[0010] Therefore, there is a need to overcome the difficulties set forth above and others previously experienced.

BRIEF DESCRIPTION OF THE INVENTION

[0011] In one implementation, probe located transceiver circuitry for ultrasound transducer elements includes a transmit section and a receive section. The transmit section includes a transmit section input, a transmit section output, and receive signal blocking circuitry coupled between the transmit section input and the transmit section output. The receive section includes a receive section input, a receive section output, and transmit signal blocking circuitry coupled between the receive section input and the receive section output. The transmit section input is coupled to the receive section output. In another implementation, the transmit section input is not coupled to the receive section output.

[0012] Other systems, methods, features and advantages of the invention will be or will become apparent to one with skill in the art upon examination of the following figures and detailed description. It is intended that all such additional systems, methods, features and advantages be included within this description, be within the scope of the invention, and be protected by the accompanying claims.

BRIEF DESCRIPTION OF THE DRAWINGS

[0013] The components in the figures are not necessarily to scale, emphasis instead being placed upon illustrating the principles of the marking systems and methods. In the figures, like reference numerals designate corresponding parts throughout the different views.

[0014] FIG. 1 illustrates a block diagram of an ultrasound probe in communication with a host system.

[0015] FIG. 2 shows a transducer stack including an array of acoustic transducer elements that may be used in the ultrasound probe shown in FIG. 1.

[0016] FIG. 3 shows receive apertures arranged across an array of acoustic transducer elements incorporated into the ultrasound probe shown in FIG. 1.

[0017] FIG. 4 depicts the transmit apertures multiplexed with receive apertures arranged across an array of acoustic transducer elements incorporated into the ultrasound probe shown in FIG. 1.

[0018] FIG. 5 shows a distribution of forty-eight (48) transducer flex cables connected to eight (8) processing boards for connecting the array of acoustic transducer elements in the probe to signal processor on the processing boards.

[0019] FIG. 6 illustrates transceiver circuitry for multiplexing selected acoustic transducer elements between reception and transmission, while protecting the signal processors connected to the acoustic transducer elements.

[0020] FIG. 7 illustrates one embodiment of transceiver circuitry using passive circuitry for multiplexing selected acoustic transducer elements between reception and transmission, while protecting the signal processors connected to the acoustic transducer elements.

[0021] FIG. 8 shows the front side and the back side of a processing board, including suggested layout areas for the electronics carried by the processing board.

[0022] FIG. 9 depicts a block diagram of a signal processor suitable for use with the ultrasound probe shown in FIG. 1.

[0023] FIG. 10 shows narrowband beamforming circuitry in the signal processor.

[0024] FIG. 11 shows an all-pass filter cell.

[0025] FIG. 12 shows a second implementation of a cross-point controller.

[0026] FIG. 13 shows a block diagram of a digital interface for the signal processor.

[0027] FIG. 14 shows signal processors connected in a serial chain.

[0028] FIG. 15 shows a cross-point controller in the signal processor that calculates new control values for processing the four receive sub-apertures assigned to the signal processor.

[0029] FIG. 16 shows steps that the ultrasound probe shown in FIG. 1 may take to perform sub-aperture processing.

[0030] FIG. 17 illustrates steps that the ultrasound probe shown in FIG. 1 may take to perform beamforming in the probe.

[0031] FIG. 18 shows steps that the ultrasound probe shown in FIG. 1 may take to transmit and receive energy to an acoustic transducer element multiplexed between a receive aperture and a transmit aperture.

[0032] FIG. 19 shows another implementation of beam-forming circuitry for the signal processors.

DETAILED DESCRIPTION

[0033] FIG. 1 illustrates a block diagram of an ultrasound probe 100. The probe 100 includes a transducer array and backing stack 102 (the “transducer array 102”), transducer cables 104, and multiple processing boards 106 that support processing electronics. Each processing board 106 includes a memory 108 (which may include geometry RAM, encoder RAM, location registers and control registers as noted below) and signal processors 110. A location cache memory and controller 112 (e.g., a general purpose CPU, microcontroller, PLD, or the like) is also present and includes a communication interface 114. The memory 108 may be separate or included as part of the signal processor 110.

[0034] The communication interface 114 establishes data exchange with the host system 116 over the digital signal lines 118 and through the signal cable 120. In addition, the signal cable 120 includes coaxial cables 122 that connect to the processing boards 106 to carry transmit pulse waveforms to the transducer array 102 and to carry back receive signals, after beamforming, to the host system 116. In another implementation the coaxial cables 122 only carry receive signals. The probe 100 may include the connector 124, through which the probe 100 attaches to the host system 116.

[0035] An interconnection 126 may be provided to connect the transducer flex cables 104 to the processing boards 106. The interconnection 126 thereby establish electrical connectivity between the transducer flex cables 104 and the processing boards 106. The interconnection 126 may be a connector, although other implementations are also suitable.

[0036] The transducer array 102 is bonded onto the backing stack, as will be described in more detail below with regard to FIG. 2. The transducer flex cables 104 provide

electrical signal connections through the backing stack. In one embodiment, there are forty-eight (48) transducer flex cables 104, each with fifty-five (55) signal connections. Thus, the transducer flex cables 104 support transmit and receive signal connections for as many as 2640 transducer elements in the transducer array 102, although fewer are used in the implementation described below.

[0037] The interconnection 126 connects the transducer flex cables 104 to the processing boards 106. In one implementation, each processing board 106 couples to six planes of transducer flex cables 104, and thereby includes signal connections for 330 transducer elements.

[0038] The processing boards 106 may, like the flex cables 104, be formed from flex material. The processing boards 106 hold the processing electronics for the transducer array 102, including the signal processors 110 that perform beam-forming on the receive apertures in the transducer array 102. The processing boards 106 also hold the transceiver circuitry for multiplexing selected acoustic transducer elements between reception and transmission, while protecting the signal processors 110 connected to the acoustic transducer elements.

[0039] As will be described in more detail below, each signal processor 110 may handle plural receive sub-apertures, for example four, defined at selected spatial locations on the transducer array 102. The receive sub-apertures may be triangular sub-apertures that include fifteen (15) acoustic transducer elements arranged, for example, as a row of five elements above a row of four elements above a row of three elements above a row of two elements above a row of one element. Furthermore, each processing board 106 may include six (6) signal processors. Thus, in the receive direction, each processing board 106 may process up to twenty (24) receive sub-apertures, each including fifteen acoustic transducer elements.

[0040] For every ultrasound beam, the cache memory and controller 112 connects over digital signal lines 132 (e.g., carried by a separate flex cable) to each signal processor controller 108 on each processing board 106. The signal processor controller 108 are drawn as a separate block labeled ‘memory’ on the processing board 106, but may also be included as part of the signal processor 110. The cache memory and controller 112 transfers static and dynamic probe setup information to the signal processor 110. Static setup information is typically spatial element locations, power settings, and delay setting mapping tables. Dynamic information is typically directional information for the sub-apertures that vary from beam to beam. The digital signal lines may include, for example, a clock line for each processing board 106, a serial command data line for each processing board 106, one or more data lines connected to each processing board 106, an output enable for one or more of the signal processors 110, and a test signal.

[0041] The cache memory and controller 112 communicates with the host system 116 over the digital signal lines 118 that may form part of a synchronous serial port, for example. To that end, the communication interface 114 and digital signal lines 118 may implement a low voltage differential signal interface, LVDS, according to the TIA/EIA-644 and IEEE 1592 standard, for example, including a coaxial cable with a grounded shield and center signal wire. The cache memory and controller 112 includes a block of

cache memory **132**, for example, 1-64 MBytes of static random access memory (SRAM).

[0042] The main purpose of the cache memory **132** in the cache memory and controller **112** is to keep beam dependent setup information for the sub-apertures. In one implementation this may be directional setup information for the sub-apertures. This is typically divided into pages where each page contains the signal processor **110** setup information required in relation to each shot. By loading up the cache pages with information for all shots in a scan sequence, this information is available in the probe during scanning. During scanning the probe setup information in relation to each shot can then be made available to the signal processors by transferring the relevant cache memory pointer to the cache memory and controller **112**.

[0043] In one implementation, the cache memory in the cache memory and controller **132** is organized into of 512 k words×16 bit (8 Mbit) and divided into pages of 128 words. The cache memory pointer can be set to the start of each page. The cache memory pointer may be, for example, a 12 bit pointer that may address a total of 4096 pages. When the cache memory **132** is a 4 Mbit cache, the cache memory pointer may be an 11 bit pointer to index 2048 pages. The words of a cache page are employed when writing or reading data to or from a chain of signal processors **110**. The digital data lines for the signal processors **110** on each processing board may be chained through shift registers over a series of plural signal processors **110**. Thus, data transferred to the signal processors **110** propagates serially through the signal processors **110**. The bit from the word with the lowest address in a page will end in the LSB bit of the shift register to the last signal processor **110** in a chain when loading data. Further, the cache memory **132** is shown within the cache memory and controller **112**, but in alternate implementations the cache memory **132** may be separate from the cache memory and controller **112**. The cache memory may also be part of the signal processors **110**.

[0044] The probe **100** response to e.g. sixteen bit commands from the host system **116**. One exemplary set of commands is shown below in Table 1. Four bits in the command may be used to define the command, while twelve bits may be used as parameters for the command.

TABLE 1

Name	Parameters Bit: 11-0	Description	Details
WR_CTRL_REG	control registry setting	Write to control/status register	cache memory and controller register
WR_CACHE_PTR	11/12 bit pointer	Set cache page pointer	The cache pointer indicates the start of the next page which will be loaded from cache memory and into the signal processors 110 .
WR_CACHE		Write a page from the host system 116 to the cache memory 132 .	The address pointer might be automatically incremented For each word written.

TABLE 1-continued

Name	Parameters Bit: 11-0	Description	Details
LD_SCAN_PAR		Write scan parameter page to signal processor 110 chain.	Updated for each ultrasound shot.
LD_CONFIG		Load memories or registers in the signal processors 110 .	Static configuration data.
DELAY_TUNE	None	Start delay calibration	Each signal processor 110 has an internal circuit to calibrate the delays
SAP_RESET	What to reset		
RD_CTRL_REG	Control register value returned	Read from control/status register	This register is internal to the cache memory and controller 112 .
RD_CACHE_PTR	Pointer value returned	Read cache page pointer register	Useful for test and verification.
RD_CACHE	None	Read a page from cache memory 132 .	The address pointer might be automatically incremented for each page read. E.g. through loop back from last signal processor 110 in chain.
RD_CONFIG		Read setup from signal processor 110 .	
CMD_ENABLE	ID code	To enable and disable command execution.	

[0045] The purpose of the command set it to control the probe. The commands may control the cache memory and controller **112** and/or the signal processors **110**. It is also desirable to include a protect mechanism to avoid undesired command execution due to noise, e.g. from the transmit pulses.

[0046] The Write Cache Pointer (WR_CACHE_PTR) command writes to the memory cache pointer register. In one implementation the parameter is a 12 bit cache pointer. The specified cache pointer is employed in the parameter field of the command when reading/writing the cache memory **132**. During read/write of cache words the cache pointer might be automatically incremented. After transfer of a full page, the pointer will thus point to the start of next page. If more than 8 MBit are used, transfer of a longer cache pointer than 12 bit can be implemented as two commands.

[0047] The Write to Cache (WR_CACHE) command loads data into the cache memory **132**. Data will be written to the cache page pointed to by the cache pointer. The cache pointer is automatically incremented after each word written to the cache. The location memory controller **112** may send a command echo when this command is received.

[0048] The Load Scan Parameters (LD_SCAN_PAR) command writes scan parameters to the signal processor **110** chain. The parameter, in one implementation, is not used. This command writes a scan parameter page to signal processors **110** from the cache page given by the cache

address pointer. This command may be triggered by the EOL signal, but may also be sent as a command.

[0049] When the data is transferred, the cache memory and controller 112 sends a calculate command to the signal processors 110 to initiate calculation of beamforming delays for the next ultrasound shot (using previous loaded setup values to save setup time). The cache memory 132 pointer is automatically incremented after each word that is written to the signal processors 110. The size of a scan parameter page may be, for example, 128 words. The word with the lowest address will end up in the LSB bit in the shift register in the last signal processor 110 in a chain.

[0050] The Load Configuration (LD_CONFIG) command loads the static setup information to the signal processor 110. Static setup information is typically spatial element locations, power settings, and delay setting mapping tables inside a signal processor 110. Each time the command is used one cache page is written to the selected memory. Some loads may require more than one cache page.

[0051] Within the signal processor the Geometry RAM holding the spatial element location may be implemented as 64 words, each 12 bits in length. The Encoder RAM holding the delay-mapping table may be implemented as 1024 words, each 5 bits in length. The start address is taken from cache memory 132 address pointer. After each page, the address pointer is incremented to next cache page. Subsequent pages may thus be loaded without updating the address pointer. The word with the lowest address in a page is the first data clocked into the signal processor 110 chain. Thus, the content of the lowest address will end up in the LSB bit of the shift register of the last signal processor 110 in the chain of signal processors 110 on a particular processing board 106.

[0052] The Initiate Delay Tuning (DELAY_TUNE) command initiates the process of calibrating the internal delays in the signal processors 110. The parameter need not be used. The result is written to the analog multi-purpose register present in the signal processor 110.

[0053] The SAP Reset Command (SAP_R_SET) command resets all the internal functions or address counters in a signal processor 110. The parameter may specify a bit pattern that selects between resetting the entire signal processor 110 or sub functionality only.

[0054] The Read Control Register (RD_CONTROL_REG) command reads the control register inside the location memory controller 112. The register content may be returned in the parameter field of the command.

[0055] The Read Cache Pointer (RD_CACHE_PTR) command reads the cache memory 132 pointer register. The value read from the cache pointer register may be returned in the parameter field of the command before the command is echoed back to the host system 116.

[0056] The Read Cache (RD_CACHE) command reads data from the cache memory 132 to the host system 116. Once the command is received the location memory controller 112 may send data words as a continuous sequence of words.

[0057] The Read Configuration from SAP (RD_CONFIG) command reads configuration data from the signal processors 110 specified by the parameter bits Configuration data

is read from the signal processors 110 and placed in the cache memory 132 in the cache page pointed to by the cache pointer. The cache address is incremented for each word read. The first word is placed in the lowest cache address. The cache address is adjusted to the start of next page when finished.

[0058] The Command Enable (CMD_ENABLE) command enables or disables command execution. After loading of scan parameters from the cache memory 132 command execution is disabled after the command is finished. Nevertheless, while disabled, the location memory controller 112 may still respond to the command enable command and the read control register command. A unique bit pattern may be added to the parameter field to reduce the possibility for this command to be generated from noise present on the command line.

[0059] As an overview, the following steps occur during scanning. First, an EOL signal (end of receiving data from previous ultrasound shot) triggers the cache memory and controller 112 to send a calculation command to signal processors 110, then transfer of a new page from the memory cache 132 to the signal processors 110. A page pointer register in the cache memory and controller 112 holds the start address for this new page. Prior to each upload the system host 116 sends the page pointer for the next ultrasound shot down the digital signal lines 118 to the cache memory and controller 112. When the page load is finished, an acknowledge signal might be sent back to the system host 116. The system host 116 then fires the ultrasound shot and acquisition of ultrasound data continues. When acquisition of the current shot is finished, the location memory controller 112 receives a new EOL and the process starts over again.

[0060] When the probe 100 is connected to the host system 116, the host system 116 transfers the setup information for each aperture and each beam into the SRAM on the location memory controller 112. The receive beamforming is split between the host system 116 and the probe 104. The host system 116 is responsible for the beamforming delay, aperture expansion, and amplitude apodization of the system receive channels driven by the signal processors 110 on the receive aperture outputs.

[0061] The signal processors 110 perform the beamforming on the individual receive sub-apertures. In one implementation, groups of fifteen transducer elements, arranged as triangular receive sub-apertures, are coupled to the signal processors 110. The signal processors 110 apply a delay to each of the receive signals arising from each of the transducer elements. The signal processors 110 also add the fifteen receive signals together and drive the aperture sum back to the host system 116 over the receive aperture outputs and the coaxial cables 122.

[0062] In one implementation using phase delays, each signal processor 110 includes, for each receive sub-aperture, fifteen (15) low noise amplifiers, fifteen (15) phase inverters, a capacitor switching network, and a two phase shifter that applies a 90 degree differential phase shift. In this embodiment the differential phase shift is wideband. The switching network applies weighting factors to the potentially inverted receive signals for summation into the phase shifters. In another implementation the signal processor are based on a delay line chain.

[0063] During operation, each signal processor 110 is configured so that the beamsteering for each receive sub-aperture points toward a focal point selected by the host system 116. To this end, the signal processor 110 determines the beamforming phase shifts based on the transducer element position within the receive aperture, the steering direction, and the receive frequency. Note that each receive sub-aperture need not use the same focal point and that receive sub-apertures farther away from the center of the transducer array 102 may be turned on later to achieve dynamically increasing aperture sizes.

[0064] The configuration of the signal processor 110 occurs in two steps. First, during probe 100 initialization, the host system 116 loads static signal processor setup information via the cache memory and controller 112 into the signal processor 110. This static information includes the geometry information, i.e., the spatial (x,y) location of the transducer elements in each receive sub-aperture and a frequency dependent translation table. Second, prior to scanning the dynamic setup information is transferred to the cache memory 132 in the cache memory and controller 112. Each one of these cache pages contains steering parameters for all sub-apertures in the probe in relation to one shot. In another implementation more than one cache page could be used to transfer the required beam related setup information.

[0065] During scanning, the host system 116 provides a beam index to the cache memory and controller 112. In response, the cache memory and controller 112 transfers the appropriate steering parameters from its cache memory to the signal processors 110. The signal processors 110 then determine beamforming delays based on the transducer element positions, the steering direction (as represented by the direction parameters). For the implementation using phase delays, the delays are converted to phase settings using the frequency dependent translation table.

[0066] Turning next to FIG. 2, that figure shows one implementation of the transducer array 102. The transducer array 102 includes piezoelectric ceramic 202 that converts electrical-to-acoustic and acoustic-to-electrical energy. The piezoelectric ceramic 202 is located within the center of the transducer array 102. On the signal side, the piezoelectric ceramic 202 is attached to a z-axis backing layer 204 with transducer flex cables 104.

[0067] The transducer flex cables 104 provide for high density signal connection. The ceramic 202, an electrically conductive inner acoustic matching layer 210, and the top surface of the backing block 204 form discrete acoustic elements 212 centered over each of the flex circuit traces 206 in the transducer flex cables 104. Thus, there is a signal plane 213 on the z-axis backing block 204.

[0068] Each circuit trace 206 contacts the bottom, or signal side, of one transducer element 212. This diced matching layer 216 is attached to the top of each element 212 to form a ground connection across the transducer array 102 face.

[0069] With regard next to FIGS. 3 and 4, FIG. 3 shows receive sub-apertures arranged across an array of acoustic transducer elements 300 incorporated into the ultrasound probe shown in FIG. 1. Similarly, FIG. 4 shows the transmit sub-apertures for one row, multiplexed with certain receive apertures arranged across the array of acoustic transducer

elements 300. The other rows shown also contain transmit elements. In one embodiment, the array includes 55 transducer elements in the lateral direction and 48 elements in the elevational direction.

[0070] However, in the implementation described below, the corners of the array are omitted which gives the array 300 an octagonal shape. All of the transducer elements, grouped into fifteen element receive sub-apertures, are used in the receive direction as shown in FIG. 3. All transmit elements, grouped into four element transmit sub-apertures are also used in the transmit direction as shown in FIG. 4.

[0071] With reference specifically to FIG. 3, each signal processor 110 combines the fifteen receive signals arising from the fifteen transducer elements for each receive sub-aperture into a single system receive channel. The signal processor 110, as noted above, applies a delay to each receive signal before summing the receive signals. The groups of 15 transducer elements form triangular apertures as indicated in FIG. 3. Thus, the overall transducer receive aperture includes 160 sub-apertures including $160 \times 15 = 2400$ transducer elements. In other embodiments, the numbers of receive sub-apertures and the numbers of transmit sub-apertures chosen depend on the number of system channels available for transmit and receive, the desired aperture size and shape and the transducer elements size.

[0072] As shown in FIG. 3, with respect to the enlarged receive aperture 48, each receive aperture is formed on a 5 by 5 grid of transducer elements. The receive aperture includes a first row of five transducer elements (labeled 11-15), a second row of four transducer elements (labeled 7-10), a third row of three transducer elements (labeled 4-6), a fourth row of two transducer elements (labeled 2-3), and a fifth row of one transducer element (labeled 1). Each transducer element has a location x_n, y_n within its sub-aperture. For example, transducer element 14 is located at $x_n=3, y_n=0$. The receive apertures are interlocked such that the combination of two receive apertures forms a rectangular patch of 5 transducer elements in lateral and 6 transducer elements in elevational direction.

[0073] With respect to FIG. 4, the shown part of the transmit aperture includes 324 transducer elements along the fifth (5) row of receive elements of the array 300. The transmit elements are grouped into 2×2 element transmit sub-apertures and each one of the transmit sub-apertures is connected to one of the system transmit channels that are carried back to the host system 116 on the coaxial cables 122. FIG. 4 shows the transmit sub-aperture 168 enlarged, including a first row of two transducer elements (labeled 3-4) and a second row of two transducer elements (labeled 1-2). The staggering of the transmit sub-apertures in the lateral (horizontal) direction is done to reduce transmit grating lobes.

[0074] In the elevation direction, three of the 2×2 transmit sub-apertures are aligned with six receive transducer elements. In the elevation (vertical direction) the overall array 300 is divided into eight groups of six rows of transducer elements each. The arrangement of the transmit and receive sub-apertures sets up the electronics partitioning. More specifically, each group of six element rows (e.g. the one labeled a-f in FIGS. 3 and 4) is connected to one processing board 106 by six transducer flex cables 104. Because no receive sub-aperture or transmit sub-aperture crosses over

the partition boundary (onto two or more processing boards), the processing electronics associated with every transducer element in the six rows are entirely contained within a single processing board 106. One significant advantage is that there is no need to route analog signals from one processing board 106 to another.

[0075] FIG. 5 illustrates a distribution 500 of forty-eight (48) transducer flex cables 104 emerging from the backing stack 204 of the transducer array 102. Six transducer flex cables 104 connected to each of eight (8) processing boards 106. The transducer flex cables 104 thereby connect the array 300 of acoustic transducer elements to the signal processors (two of which are illustrated as elements 110) on the processing boards 106. Spacers 504 may be placed in between the processing boards 106 to give desired spacing.

[0076] Each transducer flex has a connection that provide signal paths for fifty-five (55) transducer elements to connect to a particular processing board. To that end a connector is provided to couple the signals from the transducer flexes 104 to the processing board 106. There are eight such processing boards 106 in the implementation described in this document. Thus, eight processing board 106, as indicated in FIG. 5, are stacked to create a complete distribution of forty-eight transducer flex cables 104 to the processing boards 106.

[0077] FIG. 6 shows a probe circuitry for multiplexing selected acoustic transducer elements between reception and transmission, while protecting the probe electronics for transmit and receive. The implementation 600 uses the coaxes 606 to the system for both transmit and receive. In this implementation the probe receive processing circuitry 604 must have protecting circuitry both on input 603-604 connection, and on its output 602-604 connection. In another implementation with transmit circuitry in the probe 601, only the receive circuitry input, the 603-604 connection, must be protected. In this implementation the transmit circuitry need are controlled from the system over the lines 608, or from the probe cache memory and controller 112.

[0078] The multiplexing circuitry 602 and 603 may be implemented using switches or passive circuitry. An embodiment with active switches, the control circuitry must be timed relative to the signal flow. An embodiment using passive circuitry, as shown in FIG. 7, is protecting the probe circuitry based on the signal levels only. For all embodiments the multiplexers or switches used must withstand the high voltage transmit voltage, typically in the range from 10 to 400 volt peak-to-peak for piezoelectric transducer elements. For other types of transducer elements, other voltage ranges may be used.

[0079] FIG. 7 shows a passive implementation of a transceiver circuitry 700 for multiplexing selected acoustic transducer elements between reception and transmission, while protecting the signal processors connected to the acoustic transducer elements. The transceiver circuitry 700 includes multiple transmit sections, one of which is labeled 702 that incorporates a transmit section input 704, a transmit section output 706, and the two sets of receive signal blocking circuitry disposed between the transmit section input 704 and the transmit section output 706. As shown in FIG. 7, the receive signal blocking circuitry includes the back-to-back diode D1; and the back-to-back diode D3 coupled to the capacitor Cshunt.

[0080] The transceiver circuitry 700 also includes multiple receive sections, one of which is labeled 708 that incorporates a receive section output 710, a receive section input 712, and two sets of transmit signal blocking circuitry disposed between the receive section input 712 and the receive section output 710. The transmit signal blocking circuitry includes the capacitor Ccoupl connected to the diode D2; and the back-to-back diode D4 connected to the capacitor C2. The receive section inputs 712 are receive signal connections that transport receive signals obtained from the transducer elements to the signal processor 110.

[0081] The acoustic transducer elements are coupled to the transmit section output 706 and the receive section input 712. The transmit section output 706 and the receive section input 712 are connected together at the transducer elements, one of which is labeled E in FIG. 7. Similarly, the transmit section input 704 and the receive section output 710 are connected together. The receive section output 710 acts as a receive sub-aperture output driven by the signal processor 110 in the receive direction. The receive sub-aperture output thus carries a signal obtained over a receive sub-aperture, for example, a beamformed receive signal formed from receive signals obtained from 15 transducer elements in a triangular receive sub-aperture.

[0082] Note that each transmit section 702 is coupled to four transducer elements E through four diodes D1. The four transducer elements form the 2x2 transmit sub-aperture explained above. Similarly, fifteen transducer elements E are combined and summed into one receive sub-aperture output channel. Each of the fifteen receive section inputs 712 for a given receive sub-aperture includes the capacitor Ccoupl and diode pair D2. On the output side, each of the receive section outputs 710 for the combined signal obtained over the receive sub-aperture includes the diode pair D4 and the capacitor C2.

[0083] The transceiver circuitry 700 permits the transducer elements E to be multiplexed between signal reception and signal transmission while protecting the inputs and outputs of the signal processor 110. In other words, any given transducer element E may be employed to both transmit acoustic energy and receive acoustic energy.

[0084] It might not be desirable to multiplex every transducer element E, however. If some of the transducer elements in the array 300 are used for reception only, a transducer element E need not have a transmit section 702 coupled to it. This is shown in FIG. 7 and the receive only elements labeled 714 and 716. Furthermore, the transmit signal blocking circuitry may be omitted for a receive only transducer element. Similarly, a transducer element E employed only in the transmit direction need not have a receive section 708 coupled to it, nor include the receive signal blocking circuitry. Thus, for example, the receive signal blocking circuitry labeled 718 (as well as Ccoupl and D2) may be omitted for a transmit only channel.

[0085] In operation, the transmit signal (e.g., a 100 volt pulse) coming from the host system 116 passes through the diodes D3, the L_{tuning} inductor tuning and the diodes D1 to drive the transducer elements E. After the tuning inductor, the transmit signal splits into four signals and passes through four sets of D1 diodes to the four transducer elements that make up a 2x2 transmit sub-aperture.

[0086] As shown in FIG. 7, the diodes D1, D2, D3, D4 appear as antiparallel pairs. The voltage drop on the diodes

is small compared to the transmit voltage and do not have a significant impact on the transmit signal during transmit. The tuning inductor is selected to provide a voltage step-up to the transducer elements E. The resonance frequency of that circuit (i.e., the tuning inductor and the effective capacitance) is tuned to match the desired transmit frequency. The effective capacitance is formed by the parallel components of transducer element, the parasitic shunt capacitance and the coupling capacitor C_{coup} .

[0087] The coupling capacitor C_{coup} protects the signal processor **110** inputs from the transmit signal voltage. The signal processor **110** includes the internal clamping diodes **D2** which provide the current to charge the coupling capacitor to the transmit voltage. Thus, the coupling capacitor takes up nearly all of the transmit voltage, while the diodes **D2** hold the voltage present at the signal processor **110** input at plus or minus one diode drop (e.g., 0.7 V).

[0088] Because the coaxial cables **122** mainly are used for both transmit and receive, the transmit waveform would also appear (without the transmit blocking circuitry) at the signal processor **110** output. The capacitor C_2 and diodes **D4** protect the signal processor **110** output from the transmit voltage. Specifically, **D4** clamps the signal to one diode drop while C_2 decouples the signal processor **110** output from the transmit waveform by taking up the majority of the transmit voltage. The transmit waveform is sufficiently filtered by the coaxial cable **122** to limit the charge current for the capacitors C_2 and C_{coup} .

[0089] During receive, the receive signals from the transducer elements E pass through C_{coup} to the signal processor **110**. The signal processor **110** input stage is a charge amplifier A with gain determined by C_{coup} . In general, for a good noise figure, the impedance of the coupling capacitor should be small compared to the impedance of the transducer element E. However, a small impedance value increases the charge current during transmit.

[0090] Because the voltage on the transducer element is small during receive, the diodes **D1** are open. The diodes **D1** thus operate as a low voltage signal blocker to decouple the transducer elements E from each other. The echo signals received from the transducer elements are delayed and summed inside the signal processor **110** and provided to the receive section output **710**. More specifically, the output signal passes through the output resistor R and the capacitors **C1** and **C2** to the coaxial cable **122**. The load from the host system **116** preamplifier and the coaxial cable **122** capacitance is large enough to limit the output voltage at **D4** to be less than the diode on-voltage. Thus, the diodes **D4** are open-circuit during receive.

[0091] The resistor R effectively controls the signal gain into the coaxial cable **122**. The value of the protection capacitor **C2** (similar to the input coupling capacitor) is a trade-off between transmit surge current and receive impedance. In one implementation, the capacitor **C2** is approximately 100 pF. The capacitor **C1** decouples the output DC level from the clamping diodes **D4**. The precise value for **C1** is not critical, but may be set to be several times the value of **C2** (e.g., 1 nF) in order to avoid signal reduction due to **C1**.

[0092] The shunt capacitor **Cshunt** reduces the crosstalk from the receive section output **710** back to the receive section input **712**. More specifically, even though the diodes

D3 are in the off state during receive, their parasitic capacitance in the pF range will create crosstalk. The shunt capacitor is large compared to the parasitic capacitance and presents a much lower impedance than the parasitic capacitance. As a result, the diode **D3** and shunt capacitor create a voltage divider where the majority of the voltage drops off at the parasitic capacitance, while the shunt capacitor takes only a small voltage drop. Thus, the small voltage on the shunt capacitor effectively limits cross talk. Note that during transmit, when the diodes are essentially short-circuits, the shunt capacitor is a negligible load compared to the coaxial cable **122** capacitance.

[0093] FIG. 8 shows the bottom layer **802** and top layer **804** side of a processing board **106**. FIG. 8 shows an exemplary layout plan for the processing electronics included on each processing board **106** as described in detail above with regard to FIG. 7. As shown in FIG. 8, the signal processors **110** may occupy the central area of the processing boards, while the **D1** diode arrays may be located below the signal processor **110** and the **D3** and **D4** diode arrays may be located above the signal processors **110**.

[0094] Turning next to FIG. 9, that figure shows a block diagram **900** of a signal processor **110**. The signal processor **110** includes four aperture processors **902**, **904**, **906**, and **908**, a digital control block **910**, and support circuitry that may include a delay tuning circuit **912**, a recovery voltage circuit **914**, and a bias circuit **916**.

[0095] Each aperture processor **902-908** includes sixteen receive inputs (e.g., **s0In0**-**s0In15**) that are connected to transducer elements that form a receive sub-aperture. In one embodiment, the receive sub-aperture is triangular and formed from fifteen transducer elements. Thus, one input on each sub-aperture processor **902-908** may go unused. Each sub-aperture processor **902-908** also includes a test input (labeled **testin**) and digital control inputs (labeled **pgm**). The sub-aperture processors **902-908** perform beamforming on the receive input signals and output the beamformed signal obtained over the receive sub-aperture on the receive sub-aperture outputs (labeled **s0Out**-**s3Out**).

[0096] The digital control block **910** includes clock (**sClk**, e.g., a 20 MHz system clock), data (**sDataIn0** and **1**, serial data inputs and **sDataIn**, a serial control data input), and control (**sOEN**, an output enable for the signal processor **110**) signals. The digital control block also includes two data outputs (**sDataOut0** and **1**). The data inputs and outputs may be used to chain signal processors **110** in series as noted below.

[0097] The circuitry in the signal processor **110** is described in more detail below with regard to FIG. 10. FIG. 10 shows the narrowband beamforming circuitry in the signal processor **110**. Each receive input (one of which is labeled **sxIn0**) passes through a low-noise amplifier **1002**, a weighting and summation stage including mixers (one of which is labeled **1004**), summers (a positive summation summer labeled **1005** and a negative summation summer labeled **1006**), and all-pass filters **1008** and **1009**. In addition the all-pass filters connect to second summers (one of which is labeled **1010**) and through a line driver **1012** out to the receive sub-aperture output (one of which is labeled **sxOut**).

[0098] The low-noise amplifiers (LNA) are charge sensitive amplifiers that amplify the receive signal from a trans-

ducer element via the external coupling capacitor. The LNA gain may be set by adjusting the ratio between the external coupling capacitor and an internal feedback resistor. Typically the open loop gain for the LNA is high, while typical closed loop gain (at 3 MHz) is selected to exploit the available signal range.

[0099] The LNAs have fast recovery time in part due to the recovery voltage circuit **914**. If the receive signal voltage drive the circuitry into saturation recovery circuitry is activated to ensure fast recovery from the input stage saturation.

[0100] As shown in **FIG. 10**, Inphase (I) and Quadrature (Q) signals are generated from the receive signals. To that end, each input is given weight and sign depending on the desired channel delay before all the inputs are summed. A multi-input amplifier does the weighting and summing by employing individually selectable input capacitor sizes on each input. A fully differential amplifier may be employed for the summation. The sign of each input is set by feeding the input either to the positive summation node **1005** or negative summation node **1006**.

[0101] In one embodiment, the signal processor **110** uses the following weights shown in Table 2 and Table 3 for 22.5-degree quantization.

TABLE 2

Phase	IMx	qMx
0 <= phase < Pi/2	1	1
Pi/2 <= phase < Pi	-1	1
Pi <= phase < 3Pi/2	-1	-1
3Pi/2 <= phase < 2Pi	1	-1

[0102]

TABLE 3

Phase	In	qn
0	1	0
pi/8	0.924	0.383
pi/4	0.707	0.707
3Pi/8	0.383	0.924
Pi/2	0	1
X	0	0

[0103] The summation stage **1010** may further include an attenuation to level the signal swing of the available range.

[0104] The all-pass filters impart, to the I and Q signals, phase delays chosen to minimize differential phase error over a frequency band of interest. Each filter has a first-order transfer function given in the s-plane by $H(s) = (1-st)/(1+st)$, where t is the RC time constant of the filter. The transfer function may be realized using resistors and cross-coupled capacitors with active feedback. More specifically, the all-pass filters may be implemented as a non-inverting buffer followed by a resistor, in parallel with an inverting buffer in series with a capacitor (See **FIG. 20**).

[0105] In one embodiment, the all-pass filter **1008** has $RC=25$ ns, and the all-pass filter **1009** has $RC=145$ ns at 3 MHz. The determination of iMx , qMx , in , and qn are described below with regard to **FIG. 15** and Table 4.

[0106] The line driver **1012** drives the beamformed receive signal back to the host system **116**. The line driver

1012 may use a opamp with a very large output stage connected as a combination of a summer and difference amplifier. In this fashion, the signal from the I and Q channels are summed and converted into a single ended output. The gain of the combined second summation stage and line driver are selected to give the desired output range.

[0107] The delay tuning circuitry **912** is included to account for variations in process and operating conditions that may alter the time constants of the allpass filters. To control the time constants, the tuning circuit **912** is included.

[0108] The bias circuit **916** controls the bias currents to the analog modules in the signal processor **110**. The power supply voltage may be used as a reference voltage. In one implementation, the bias current is distributed over the signal processor **110** to supply the different analog modules with the required bias current.

[0109] Turning next to **FIG. 13**, that figure shows a block diagram of the digital interface **1300** of the signal processor **110** that is included in the digital control block **910**. The digital interface **1300** includes four pairs of six-bit registers/memories **1302** and **1304**, **1306** and **1308**, **1310** and **1312**, and **1314** and **1316** for storing delta Y and delta X inclination parameters for the four receive apertures handled by the signal processor **110**. The digital interface **1300** also includes two 1-bit bank memories **1318**, **1320**, two data shift registers **1322**, **1324**, a multi-bit key register **1326**, and a multi-bit command register **1328**. The tri-state buffers **1330** and **1332** allow the interface **1300** to place its outputs in a high impedance state under control of the SOEN signal.

[0110] The interface **1300** may be used to program, set up and read from the signal processor **110**. The interface **1300** includes a command line (SCDATAIN), two data lines (SDATAIN0, 1), one enable line (SOEN), and one clock line SCLK (not shown). The SDATAIN0 and SDATAIN1 lines provide for serial data input to the two data shift registers **1322**, **1324** (labeled SHIFTREGISTER0, 1), while SCDATAIN provides for serial data input to a control data shift register. In one implementation, the data shift registers may be 25 bits long, while the control shift register may be 36 bits long.

[0111] The signal processor **110** is typically used in a hostile environment where the digital input lines are expected to assume random values during ultrasound-transmission. To avoid getting false data and commands through the digital interface, the 32 bit key register is used as an enable signal. When the correct key resides in the key register (compared to the key pre-selected and pre-set in the signal processor **110**), the digital controller executes the command placed in the 4 bit command register.

[0112] The data lines may be shifted simultaneously into the registers controlled by the SCLK data clock. SCLK runs, for example, at 20 MHz. Note that the interface **1300** also includes two digital outputs labeled SDATAOUT0 and SDATAOUT1. These outputs are the outputs of the data shift registers and may be used to connect multiple signal processors **110** in a chain (See **FIG. 14**). Output data from the signal processors **110** are shifted through the serial chain and read out from the last signal processor **110** in the chain.

[0113] Because the output-bus is connected to the input-bus in the chain, the SOEN signal may be employed to place the output of the last signal processor **110** in tristate mode

(Hi Z mode) when writing to the chain. When reading out data over the serial bus, SOEN may be used to enable the output from the last signal processor **110**.

[0114] In one implementation, the 36-bit control data register includes of a 32-bit key register and a 4-bit command register. The SCDAVIN line may be a separate signal line to all signal processors **110** on a processor board **106**. In addition, as shown in **FIG. 13**, the serial shift registers are shifted in from most significant bit (MSB). In other words, command and data is shift in LSB first.

[0115] Also shown in **FIG. 13** are the six bit inclination parameter memories that store location information for the four receive sub-apertures handled by the signal processor **110**. The pair of six-bit memories **1302**, **1304** store delta Y and delta X inclination information for a receive sub-aperture and the pair of six-bit memories **1306**, **1308** store delta Y and delta X inclination parameters for a second receive sub-aperture. Similarly, the pair of six-bit memories **1310**, **1312** store delta Y and delta X inclination parameters for a third receive sub-aperture and the pair of six-bit memories **1314**, **1316** store delta Y and delta X inclination parameters for a fourth receive aperture. Then loading the signal processor static information (geometry ram, setup registers, encoder ram, etc.) the shift register division is adapted to the data loaded.

[0116] Turning briefly to **FIG. 14**, that figure shows a serial chain **1400** of signal processors **110**. The serial chain **1400** is connected through the SDATAOUT0, SDATAOUT1, SDATAIN0, and SDATAIN1 signal lines. A clock line, latch line, and parameter selection line (for selecting which parameter registers to write) may also be provided.

[0117] Turning next to **FIG. 15**, that figure shows a cross-point controller **1500** in the signal processor **110** that calculates new control values for processing the four receive sub-apertures assigned to the signal processor **110** based on the delta X, delta Y inclinations loaded through the serial interface (See **FIG. 13**). The cross-point controller **1500** will calculate 16 new delay settings for each aperture, based on new inclinations parameters delta X, delta Y. The delay setup are calculated based on the contents of the geometry RAM and the new inclinations parameters delta X, delta Y. The corresponding phase delays are found from lockup in the chosen encoder RAM bank.

[0118] To that end, the cross-point controller **1500** includes the multipliers **1502**, **1504**, and a summer **1505**. The cross-point controller **1500** also includes a controller **1506**, a geometry ram **1508**, and an encoder ram **1510**. Four sets (one for each receive sub-aperture) of sixteen 5-bit phase setting registers **1512**, **1514**, **1516**, and **1518** are provided (a total of 64 five-bit registers). These delay setting registers store the delay setting control bits for each receive sub-aperture handled by the signal processor **110**, as noted below.

[0119] The geometry RAM **1508** holds the relation between a receive signal channel n , and the corresponding transducer location (x_n, y_n) within the receive sub-aperture. The encoder RAM **1510** holds the relation between the coded delay and the hardware settings $(iMxn, in, qMxn, qn)$ shown in **FIG. 10** for narrowband beamforming. Alternatively, the encoder RAM **1510** holds the relation between the

desired delay and the cross-point switch control signals intPol, chPos(4), and sign for the broadband beamforming circuitry shown in **FIG. 19**. The parameter delta X_n represents the x-inclination for sub-aperture n , $n=0, 1, 2, 3$, while delta Y_n represents the y-inclination for sub-aperture n , $n=0, 1, 2, 3$ for each of four sub-apertures handled by the processor **110**.

[0120] When a valid key is detected in the key register and the start cross-point calculation command is selected, the cross-point controller **1500** calculates new register values for sub-apertures **0**, **1**, **2** and **3**. Because up to 16 receive signals may contribute to each receive aperture, a total of 64 calculations are performed. The delta X and delta Y values shown in **FIG. 15** are the values loaded from the serial interface prior to each new setup. All eight delta X and delta Y values loaded during the previous setup calculation are available to the cross-point controller **1500** via two 24 bit buses as shown in **FIG. 13**.

[0121] To save setup time, the data to be used in the next calculation is shifted in and loaded while the signal processor is calculating the current setup. When the current calculation is finished, the new delta X and delta Y data have been loaded and are ready for the next setup calculation.

[0122] To start a calculation the key and command register are loaded with the key value and the bit code assigned to the desired command. When a calculation is initiated, delta X and delta Y values for aperture **0** are put on the multiplier **1502**, **1504** inputs. A sequencer **1506** controls the calculations. The sequencer **1506** may be implemented as an up counter that cycles through all 64 receive signal inputs (4 sub-apertures times 16 receive inputs per sub-aperture). The sequencer **1506** is connected to the address bus of the geometry RAM **1508**. The data for one sub-aperture is generally calculated before advancing to the next sub-aperture.

[0123] The sequencer **1506** also controls routing the signal from the encoder RAM **1510** to the correct analog sub-aperture register **1302-1314**, as well as the multiplexing of the correct delta X and delta Y data to the cross-point controller **1500**. In one implementation for narrowband beamforming, the output from the Encoder RAM **1510** is a 5 bit word, called sap_data [4:0] that maps to sX_m_controlX().

[0124] sX_m_controlX() maps to the control signals for the beamforming circuitry shown in **FIG. 10**. The five bits sX_m_control4..0(Y) directly control the angular weight and sign to the Y channel (receive signal) for aperture X. The translation from bit values to angular weight and sign is given in Table 4. In other words, the Encoder RAM **1510**, for narrowband beamforming, maps from a delay value to the multiplexer sign (iMxn and qMxn) and the I and Q scaling (in and qn). These parameters implement 16 phase angles, and to be able to omit signals with given delays, in=qn=0 may also be selected. As a result, the word length in the Encoder RAM **1510** is 5 bits. Alternatively, the bits in the Encoder RAM **1510** may directly choose coefficients and multiplexer values (e.g., using one bit for each multiplexer, and 3 bits with decoder to select each of the six gain-pairs in Table 3).

TABLE 4

Mapping between SAP control bits and phase										
#	bit4	bit3	bit2	bit1	bit0	iMxn	in	qMxn	qn	Phase
0	0	0	0	0	0	1	1.0	X	0.0	0
1	0	0	0	0	1	1	0.924	1	0.383	Pi/8
2	0	0	0	1	0	1	0.707	1	0.707	Pi/4
3	0	0	0	1	1	1	0.383	1	0.924	3Pi/8
4	0	0	1	0	0	X	0.0	1	1.0	Pi/2
5	0	0	1	0	1	-1	0.383	1	0.924	5Pi/8
6	0	0	1	1	0	-1	0.707	1	0.707	3i/4
7	0	0	1	1	1	-1	0.924	1	0.383	7Pi/8
8	0	1	0	0	0	-1	1.0	X	0.0	Pi
9	0	1	0	0	1	-1	0.924	-1	0.383	9Pi/8
10	0	1	0	1	0	-1	0.707	-1	0.707	5Pi/4
11	0	1	0	1	1	-1	0.383	-1	0.924	11Pi/8
12	0	1	1	0	0	X	0.0	-1	1.0	3Pi/2
13	0	1	1	0	1	1	0.383	-1	0.924	13Pi/8
14	0	1	1	1	0	1	0.707	-1	0.707	7Pi/4
15	0	1	1	1	1	1	0.924	-1	0.383	15Pi/8
16 . . . 31	1	X	X	X	X	X	0.0	X	0.0	X

[0125] The calculations may be done with 2's complement number representation. Referring again to **FIG. 15**, the delta X and delta Y and geometry RAM data are multiplied and summed in the summer **1505**. This calculation produces a 13 bit output. Because delta X and delta Y are never maximal at the same time, in the calculations the two MSBs will always be the same and the MSB of the signal can be truncated. In the implementation shown in **FIG. 15**, precision is reduced to 8 bits by truncating the four LSBs.

[0126] The cross-point controller **1500** sequences through all transducer element receive inputs 'n' for every receive aperture 'm' handled by the signal processor **110**. The cross-point controller **1500** may be considered to determine a scaled version of the delay to be introduced to each receive signal as: $\text{floor}((x(m,n)*\text{delta}X(m)+y(m,n)*\text{delta}Y(m))/16)$, for $n=0, 1, \dots, 15$, and $m=0, 1, 2, 3$.

[0127] Note that $x(m,n)$ and $y(m,n)$ are the geometrical positions of the transducer element coupled to the nth input for receive aperture m. The positions are indexed through the geometry RAM **1508** to add routing flexibility during processing circuit board **106** layout. The inclination parameters $\text{delta}X(m)$ and $\text{delta}Y(m)$ may remain constant for all receive signals in a given receive sub-aperture m, but may typically vary between the sub-apertures.

[0128] The calculated delay is converted into a physical delay through a table look-up in the encoder RAM **1510**.

[0129] With regard to the geometry RAM **1508**, it takes a 6 bit address and stores 12 bit data. To start loading data to the geometry RAM **1508**, the command **RESET_ADDR_COUNTERS** is issued to reset the address counters. The next command is then **LOAD_GEOG_RAM**, which will write data to the current addresses pointed to by the address counter, and auto-increment the address counter. Because the datawidth is 12 bit, one shift/load procedure will load 4 datawords into the geometry RAM **1508**. The address counter will therefore be incremented by 4 at each load.

[0130] The encoder RAM **1510** is divided into four banks, reflecting four different frequency settings for the ultrasound probe **100**. The bank**0** and bank**1** registers loaded from the serial interface specify which bank is used. Together with

the eight bits from the calculation, they make up the encoder RAM address in the 1024x5 bit RAM.

[0131] The encoder RAM **1510** has a 10 bit address bus and a 5 bit data bus. To start loading data to encoder RAM **1510**, the command **RESET_ADDR_COUNTERS** is issued to reset the address counters. The next command is **LOAD_ENC_RAM**, which will write data to the current addresses pointed to by the address counter and bank **0/1** registers, and auto-increment the address counter. Since the data width is 5 bit, one shift/load procedure will load 8 aperture control data words to the RAM **1510**. The address counter will therefore be incremented by 8 at each load.

[0132] Bits [19:0] in both serial shift registers are used for data to the RAMs. Bit **24** of serial shift register **0** is mapped to the bank **0** control signal for the encoder RAM **1510**, and bit **24** of serial shift register **1** is mapped to the bank **1** control signal. Bank **0/1** registers (See **FIG. 13**) control which bank is loaded. In one embodiment, the location memory controller **112** sends four-bit commands to the signal processors **110**. The commands are shifted into the signal processors **110** into the command register **1328**. Exemplary commands are presented below in Table 5:

TABLE 5

Name	Command
RESET	Places the signal processor into a known state
LOAD_X_Y_Data	Load delta X and delta Y and encoder bank from shift register.
RESET_ADDR_COUNTERS	Reset all address counters for reading and writing to the signal processor.
LOAD_GEOG_RAM	Load 4 datawords to geometry RAM.
LOAD_ENC_RAM	Load 8 datawords to encoder RAM.
CALCULATE	Calculate new aperture beamforming values.
DELAY_TUNING_START	Start analog tuning and calibration procedure.
WRITE_ANALOG_MP_REG	Write to the analog multi-purpose register in the signal processor.
READ_ANALOG_MP_REG	Put the analog multi-purpose register, containing, for example, the delay measurement from the delay tuning, on the 1322, 1324.

TABLE 5-continued

Name	Command
READBACK_REGS	Read out the internal registers of the signal processor.
WRITE_REGS	Write directly to the internal registers of the signal processor.
LOAD_PD_REG	Write a analog power-down register.

[0133] FIG. 16 summarizes the steps 1600 that the ultrasound probe 100 shown in FIG. 1 may take to perform sub-aperture processing. The probe 100 receives, at signal processors 110 distributed over processing boards 106, multiple receive signals from acoustic transducer elements (Step 1602). The transducer elements may form triangular receive sub-apertures that are wholly processed by a given signal processor 110, rather than being partitioned between processing boards. During the receive (and transmit) operations, the probe 100 multiplexes at least one of the acoustic transducer elements between the receive sub-aperture and a square transmit sub-aperture (Step 1604).

[0134] After beamforming, the signal processor 110 drives a receive sub-aperture output with a beamformed signal obtained over the acoustic transducer elements in the receive sub-aperture (Step 1606). In the transmit direction, the probe may couple transmit signals to multiple transmit sub-apertures over transmit signal connections distributed between multiple processing boards (Step 1608). Like the receive apertures, the transmit signal connections for a given sub-aperture may all be provided on a given processing board 106, rather than being partitioned across multiple processing boards 106.

[0135] Not partitioning the transmit or receive sub-apertures between multiple processing boards provides for efficient routing of signals between the host system 116 and the processing boards 106 to the transducer array 102. Because each processing board 106 processes its own transmit and receive sub-apertures, no cross-connecting signals or routing needs to be provided between the processing boards 106.

[0136] FIG. 17 summarizes the steps 1700 that the ultrasound probe 100 shown in FIG. 1 may take to perform beamforming in the probe 100. The probe 100 receives multiple directional parameters such as inclination values (e.g., delta X and delta Y data) for the receive sub-apertures from a host system 116 at a cache memory and controller 112 (Step 1702). The cache memory and controller 112 then transfers the directional parameters to multiple signal processors 110 on multiple processing boards 106 (Step 1704).

[0137] The probe 100 couples to signal processors 110, receive signals arising from a receive sub-aperture (Step 1706). The signal processor 110 retrieves, from the serial input registers (e.g., 1302-1304, 1306-1308, 1310-1312, or 1314-1316), directional parameters for the receive sub-aperture (Step 1708). Based on the directional parameters, the signal processor determines a beamforming delay for the transducer elements in the receive sub-aperture (Step 1710), and applies the delay to the receive signal from each respective transducer element (Step 1712).

[0138] FIG. 18 shows steps 1800 that the ultrasound probe 100 shown in FIG. 1 (e.g., using the transceiver

circuitry 700 may take to transmit and receive energy to an acoustic transducer element multiplexed between a receive aperture and a transmit aperture.) The circuitry 700 couples a transmit pulse through a transmit section input 704, a transmit section output 706, and receive signal blocking circuitry D1, D3 and Cshunt coupled between the transmit section input 704 and the transmit section output 706 (Step 1802). The transceiver circuitry 700 also couples a receive signal through a receive section input 712, a receive section output 710, and transmit signal blocking circuitry C2 and D4, and Ccouple and D2, coupled between the receive section input 712 and the receive section output 710 (Step 1804).

[0139] Turning next to FIG. 19, that figure shows a block diagram 1900 of another implementation of beamforming circuitry in the aperture processors 902-908. The beamforming circuitry 1900 includes the pre-amplifiers 1902, one for each of sixteen receive channels in a receive aperture, and one for testing. The pre-amplifiers 1902 are connected to a 34x11 cross-point matrix 1904 that flexibly connects the receive signals through zero to ten delay elements 1906 and summing nodes 1908 that form, in series, a delay line. The line driver 1910 drives the combined signal back to the host system 116.

[0140] The cross-point matrix 1904 supports the connection of any receive channel to any node of the delay line. When several channels are connected to the same node of the delay line, then the output of that node is the sum of the respective input signals. Any channel may be inverted before entering a summing node, and any channel may optionally be simultaneously connected to two adjacent summing nodes. In that case, the signal will then split so that the effective gain is reduced by approximately 6 dB for each.

[0141] When the beamforming circuitry 1900 is employed, the cross-point controller 1500 outputs the following signals to the beamforming circuitry 1900: intPol, chPos(4).

[0142] FIG. 11 shows one implementation for an all-pass filter cell (e.g., the filter cell 1906). As shown, the all-pass filters may be implemented as a non-inverting buffer followed by a resistor R, in parallel with an inverting buffer in series with a capacitor C. Each filter cell has a phase delay of T=2RC, and a transfer function of $H_c(w) = (1-j(wT/2))/(1+j(wT/2))$.

[0143] FIG. 12 shows a cross-point controller 2100 for use with the beamforming circuitry 1900 to program the switches in the cross-point matrix 1904, starting on a trigger event and operating on the latched version of the scan parameters. The cross-point controller 2100 sequences through all transducer element receive inputs 'n' for every receive aperture 'm' handled by the signal processor 110. The cross-point controller 2100 may be considered to determine a preliminary scaled version of the delay to be introduced to each receive signal as: $\text{floor}((x(m,n)*\text{delta}X(m)+y(m,n)*\text{delta}Y(m))/8)$, for n=0, 1, ..., 15, and m=0, 1, 2, 3.

[0144] Note that x(m,n) and y(m,n) are the geometrical positions of the transducer element coupled to the nth input for receive aperture m. A reserved code may be established (e.g., x(m,n), y(m,n)=-16, -16) that disables (e.g., for power management) channel n of the aperture m by using the decoder 2102 to detect the code (or optionally or in addition,

overflow of chPos), and assert a channel disable output signal. The positions are indexed through the geometry RAM **1508** to add routing flexibility during processing circuit board **106** layout. The scale factors deltaX(m) and deltaY(m) may remain constant for all receive signals in a given receive aperture m.

[0145] The preliminary delay is converted into a physical delay through a table look-up in the encoder RAM **1510**. In one implementation, the output of the encoder RAM **1510** includes six bits: one bit for intPol, four bits for chPos, and one bit for sing. The chPos bits cause the corresponding switch in the cross-point matrix **1904** to be closed. If the control bit intPol is set, the switch 1+chPos will also be set. The sign bit selects the non-inverted or inverted version of the input signal.

[0146] While various embodiments of the invention have been described, it will be apparent to those of ordinary skill in the art that many more embodiments and implementations are possible that are within the scope of this invention.

What is claimed is:

1. Transceiver circuitry for ultrasound transducer elements, the transceiver circuitry comprising:

a transmit section comprising:

a transmit section input;

a transmit section output; and

receive signal blocking circuitry coupled between the transmit section input and the transmit section output; and

a receive section comprising:

a receive section input;

a receive section output and

transmit signal blocking circuitry coupled between the receive section input and the receive section output.

2. The transceiver circuitry of claim 1, where the transmit section output is coupled to the receive section input.

3. The transceiver circuitry of claim 1, where the transmit section input is coupled to the receive section output.

4. The transceiver circuitry of claim 1, where at least one of the transmit and receive signal blocking circuitry comprises clamping diodes.

5. The transceiver circuitry of claim 1, where the receive signal blocking circuitry comprises clamping diodes coupled to the transmit section output and back-to-back diodes coupled to the transmit section input.

6. The transceiver circuitry of claim 1, further comprising back-to-back diodes coupled between multiple transducer elements, said back-to-back diodes forming a short circuit between said multiple transducer elements during transmit.

7. The transceiver circuitry of claim 1, further comprising back-to-back diodes coupled between multiple transducer elements, said back-to-back diodes forming an open circuit between said multiple transducer elements during reception.

8. The transceiver circuitry of claim 1, where the transmit signal blocking circuitry comprises clamping diodes coupled to the receive section input and clamping diodes coupled to the receive section output.

9. The transceiver circuitry of claim 1, further comprising a voltage step up circuit coupled between the transmit section input and the transmit section output.

10. An ultrasound probe comprising:

a transducer array comprising array transducer elements; and

transceiver circuitry comprising:

a transmit section output coupled through receive signal blocking circuitry to transmit transducer elements comprising a transmit aperture;

a receive section input coupled to a multiplexed transducer element selected from the transmit transducer elements,

wherein the transmit section output drives the multiplexed transducer element during ultrasound beam transmission and where the receive section input receives a reception signal from the multiplexed transducer element during ultrasound beam reception.

11. The ultrasound probe of claim 10, where the transceiver circuitry further comprises a transmit section input coupled to a receive section output.

12. The ultrasound probe of claim 10, where the receive signal blocking circuitry comprises low level signal blocking circuitry.

13. The ultrasound probe of claim 10, where at least one of the transmit and receive signal blocking circuitry comprises clamping diodes.

14. The ultrasound probe of claim 10, further comprising transmit signal blocking circuitry coupled to the receive section output.

15. The ultrasound probe of claim 10, further comprising back-to-back diodes coupled between multiple transducer elements, said back-to-back diodes forming a short circuit between said multiple transducer elements during transmit.

16. The ultrasound probe of claim 10, further comprising back-to-back diodes coupled between multiple transducer elements, said back-to-back diodes forming an open circuit between said multiple transducer elements during reception.

17. The ultrasound probe of claim 10, where the transmit aperture comprises a rectangular patch of transmit transducer elements.

18. The ultrasound probe of claim 10, where the rectangular patch is a 2x2 patch.

19. The ultrasound probe of claim 10, where the multiplexed transducer element is included in a triangular receive aperture comprised of selected array transducer elements.

20. The ultrasound probe of claim 10, where the receive aperture comprises a first section of five transducer elements, a second section of four transducer elements, a third section of three transducer elements, a fourth section of two transducer elements, and a fifth section of one transducer element.

21. A method for transmitting and receiving signals through ultrasound transducer elements, the method comprising the steps of:

coupling a transmit pulse through a transmit section input, a transmit section output, and receive signal blocking circuitry coupled between the transmit section input and the transmit section output; and

coupling a receive signal through a receive section input, a receive section output, and transmit signal blocking circuitry coupled between the receive section input and the receive section output.

- 22.** The method of claim 21, wherein the transmit section input is coupled to the receive section output.
- 23.** The method of claim 21, where the transmit section output is coupled to the receive section input.
- 24.** The method of claim 21, where the receive signal blocking circuitry comprises low level signal blocking circuitry.
- 25.** The method of claim 21, where at least one of the transmit and receive signal blocking circuitry comprises a clamping diode and an impedance element.
- 26.** The method of claim 21, where the receive signal blocking circuitry comprises back-to-back diodes coupled to the transmit section output and clamping diodes coupled to the transmit section input.
- 27.** The method of claim 21, where the transmit signal blocking circuitry comprises clamping diodes and a capacitor coupled to the receive section output and back-to-back diodes coupled to the receive section input.

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摘要(译)

用于超声换能器元件的收发器电路包括发送部分和接收部分。发送部分包括发送部分输入，发送部分输出和连接在发送部分输入和发送部分输出之间的接收信号阻塞电路。接收部分包括接收部分输入，接收部分输出和连接在接收部分输入和接收部分输出之间的发送信号阻塞电路。

