



US 20190150889A1

(19) **United States**(12) **Patent Application Publication**
XU et al.(10) **Pub. No.: US 2019/0150889 A1**(43) **Pub. Date: May 23, 2019**(54) **AN ULTRASOUND SYSTEM AND METHOD****Publication Classification**(71) Applicant: **KONINKLIJKE PHILIPS N.V.**,
EINDHOVEN (NL)(72) Inventors: **JINGPING XU**, SHANGHAI (CN);
BALASUNDAR IYYAVU RAJU,
NORTH ANDOVER, MA (US);
SHOUGANG WANG, OSSINING, NY
(US); **MCKEE DUNN POLAND**,
ANDOVER, MA (US); **ANTHONY M.**
GADES, SNOHOMISH, WA (US)(51) **Int. Cl.****A61B 8/00** (2006.01)**A61B 8/08** (2006.01)(52) **U.S. Cl.**CPC **A61B 8/4281** (2013.01); **A61B 8/4254**(2013.01); **A61B 8/5223** (2013.01); **A61B****8/467** (2013.01); **A61B 8/4483** (2013.01)

(57)

ABSTRACT

The invention relates to an ultrasound system (100) for sequentially performing a predetermined procedure for each of at least one region of interest. The ultrasound system (100) comprises an ultrasound probe (101) configured to transmit a first ultrasound signal (SG1) towards a region of interest and receive echo signals from the region of interest. The ultrasound system (100) also comprises a motion sensor (102) configured to detect a motion of the ultrasound probe (101) and generate a motion signal (MS) for indicating the motion of the ultrasound probe (101). The ultrasound system (100) also comprises a processor (103) configured to perform a predetermined procedure for a region of interest on the basis of the echo signals received from the region of interest if the motion signal (MS) indicates that the ultrasound probe (101) is stationary. The invention also relates to a corresponding ultrasound method.

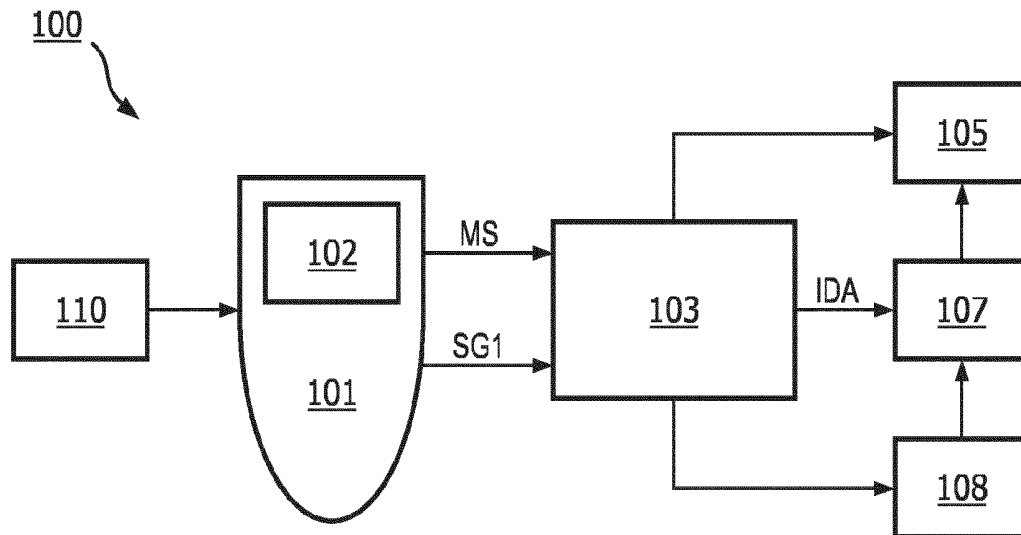
(21) Appl. No.: **16/066,723**(22) PCT Filed: **Dec. 19, 2016**(86) PCT No.: **PCT/EP2016/081629**

§ 371 (c)(1),

(2) Date: **Jun. 28, 2018**(30) **Foreign Application Priority Data**

Dec. 30, 2015 (CN) PCT/CN2015/099880

Mar. 9, 2016 (EP) 16159416.3



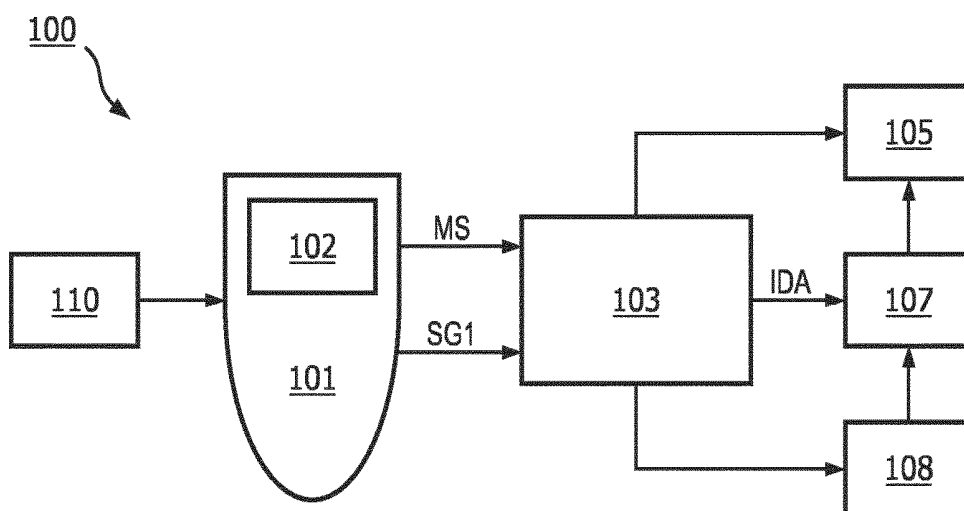


FIG. 1

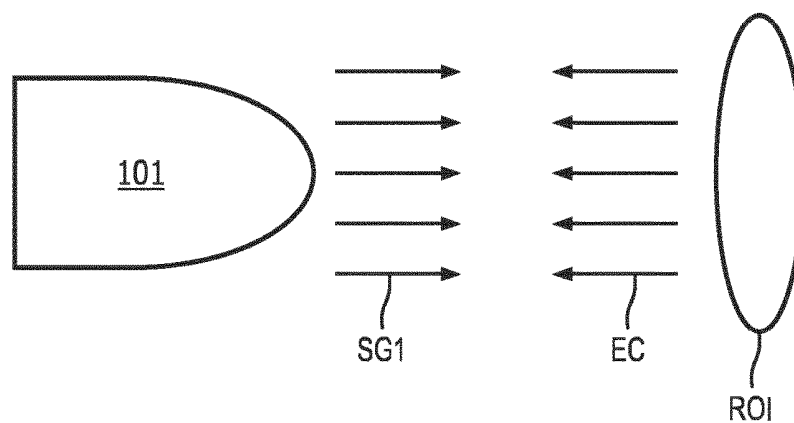


FIG. 2

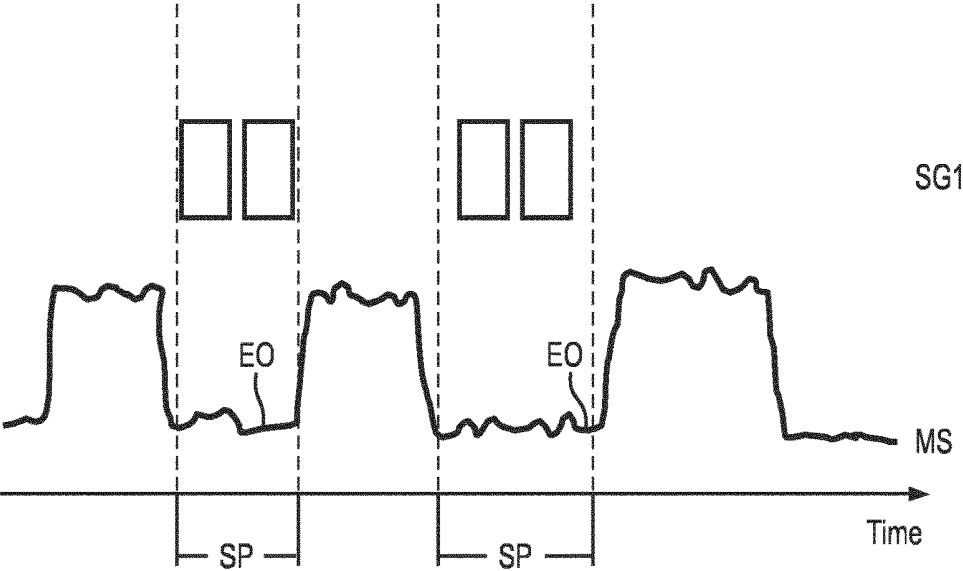


FIG. 3

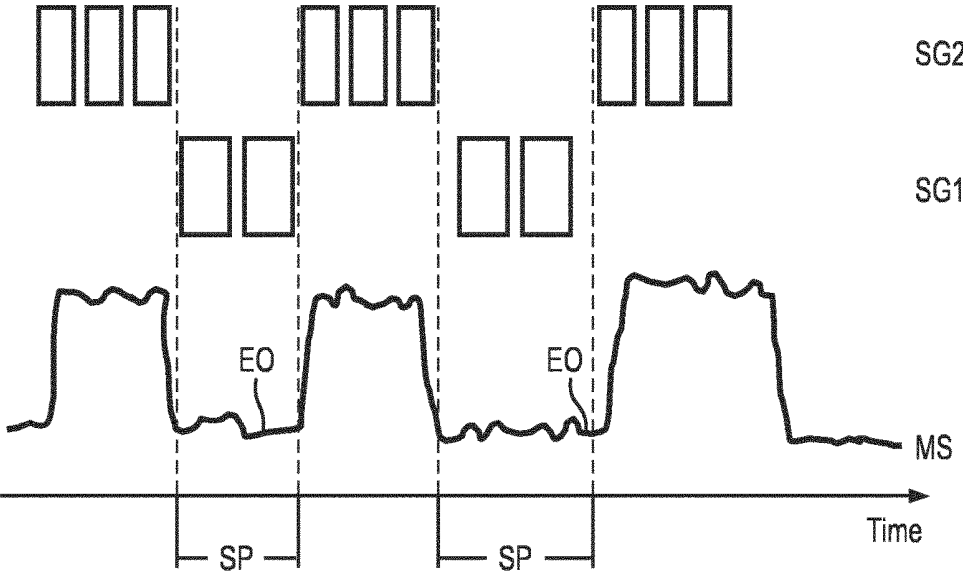


FIG. 4

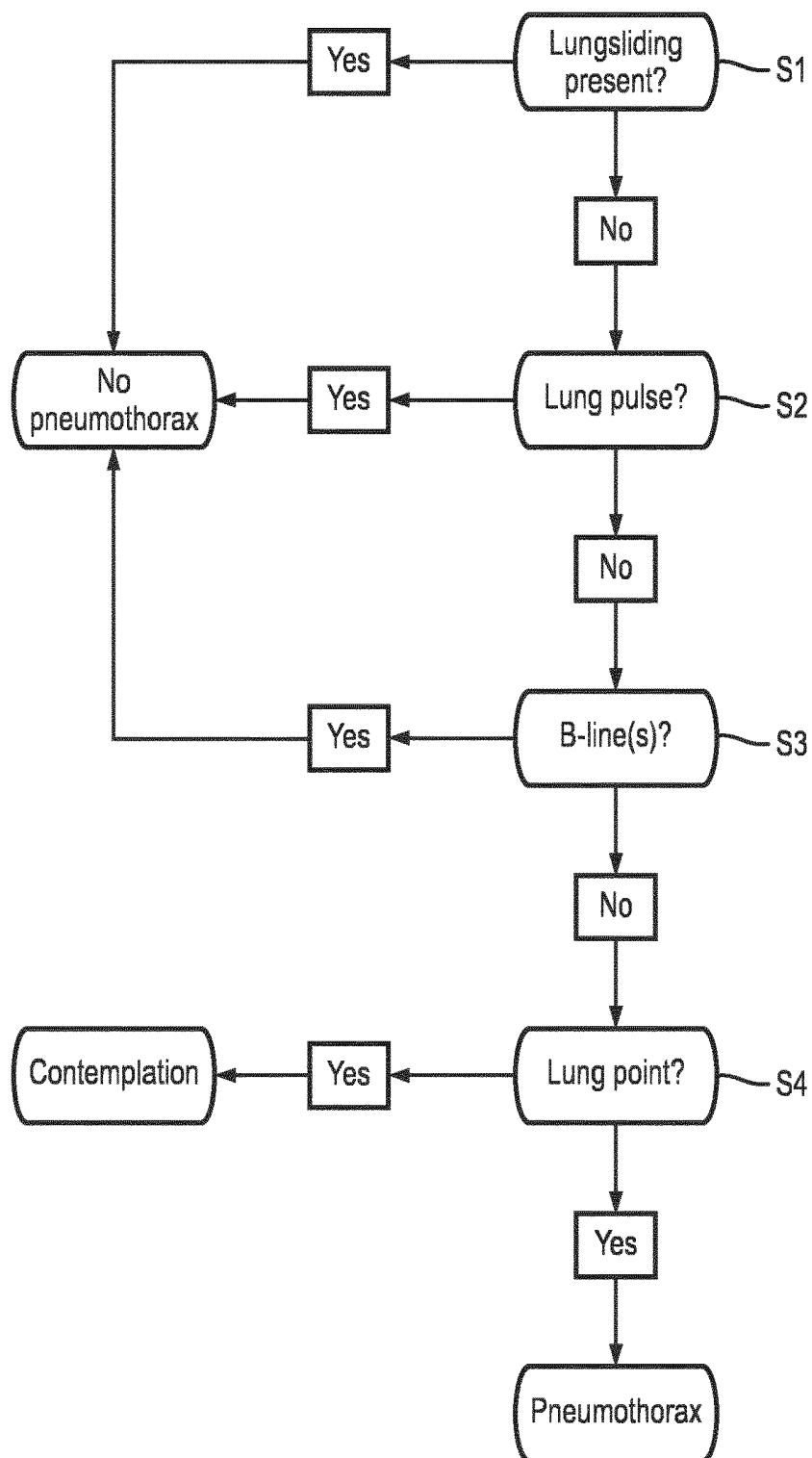


FIG. 5

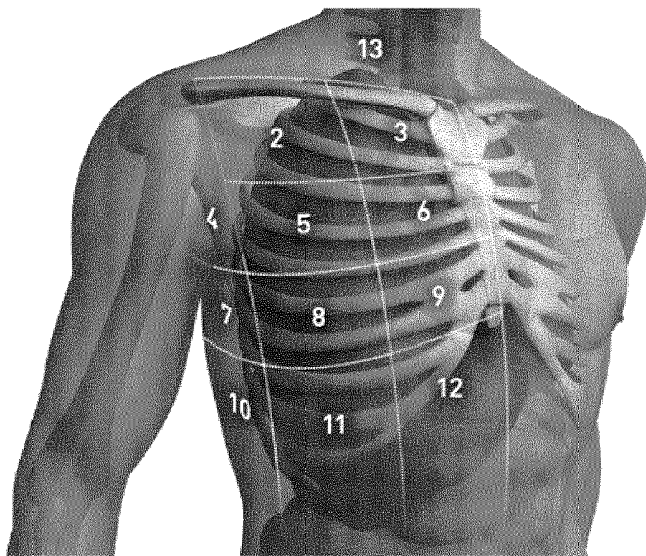


FIG. 6

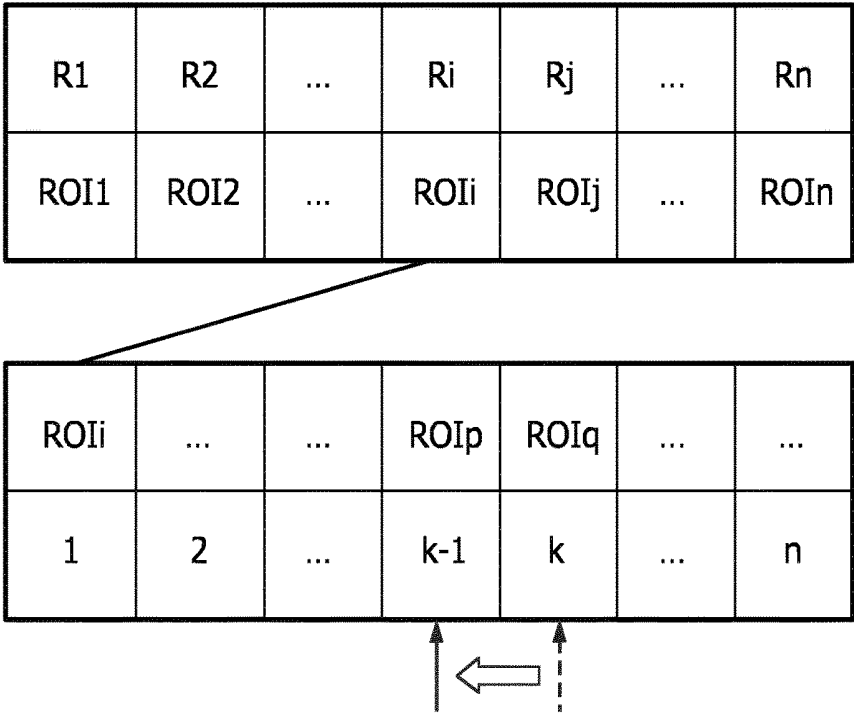


FIG. 7

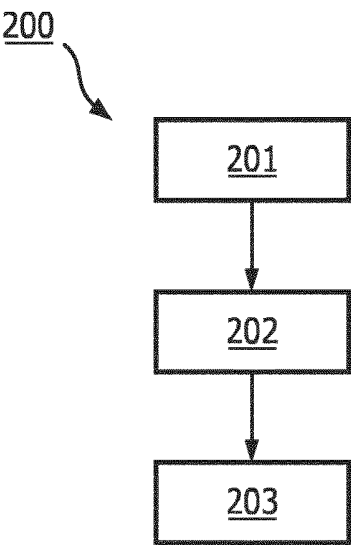


FIG. 8

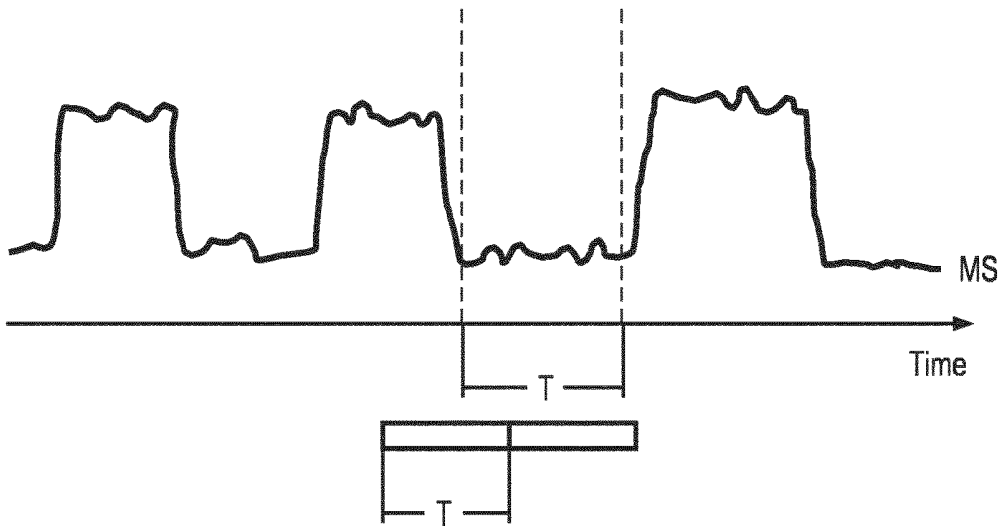


FIG. 9

AN ULTRASOUND SYSTEM AND METHOD

FIELD OF THE INVENTION

[0001] The invention relates to the field of ultrasound, in particular to a system and a method for sequentially performing a predetermined procedure for each of at least one region of interest.

BACKGROUND OF THE INVENTION

[0002] Pneumothorax (PTX) is a common problem in various settings, for example, emergency care, respiratory care, interventional radiology, critical care and anaesthesia, etc. PTX represents the second most common injury after rib fracture in the domain of blunt chest trauma. Large PTXs may cause respiratory distress, and tension PTXs may cause cardiorespiratory failure. Rapid detection of PTX is important due to the life-threatening nature of these conditions.

[0003] At present, ultrasound is widely used for detection of pneumothorax (PTX). In accordance with a certain sequence defined by the clinical protocol, an ultrasound probe will be sequentially placed at various portions of the chest to detect the presence of PTX at each portion of the chest. Based on the obtained ultrasound data of each portion, the ultrasound system can analyze the ultrasound data to extract features of each portion to rule out or rule in PTX automatically. As shown in FIG. 6, there will be more than ten portions of the entire chest to be checked to determine PTX, and it will be very time-consuming if the ultrasound system cannot timely start to analyze obtained ultrasound data to determine PTX. However, if the ultrasound system start the ultrasound data analysis too early, for example, the ultrasound probe has not moved to the next portion and then the obtained ultrasound data comprise the data obtained from two portions of the chest, the analyzed result will be fully wrong. Therefore, the balance between the efficiency and accuracy is critical for providing an ultrasound system which determines when to start PTX check on each portion of multiple portions of the chest.

[0004] There may be solutions which can partly solve the issue mentioned above. For example, assuming that the PTX determination on each portion will take at most time period T as shown in the upper part of FIG. 9, a proper long enough time period 2T is periodically reserved as shown in the lower part of FIG. 9 for the ultrasound system to do the PTX determination on each portion. For one more example, the solution can be obtaining the exact position information of the ultrasound probe by placing lots of markers on the subject and the ultrasound system will do PTX determination when the probe is detected on a certain portion based on the position information. However, the above two solutions may either be too time-consuming or too complex to be implemented.

[0005] US2007/0078340 A1 discloses a method and system for providing an operational command signal to a workstation of an imaging system. The workstation is provided imaging data from a positionable transducer. The method and system convert at least one of a predetermined plurality of motion patterns inputted by an operator of the system to the transducer into the operational command signal. However, US2007/0078340 A1 provides solutions to use several motion patterns to discriminate between motion intended to initiate control changes and motion which occurs normally during scanning, and it fails to provide applicable

solution to solve the above mentioned issue of PTX determination which involves multiple consecutive determination on human body.

[0006] US2014/0128739 A1 discloses an ultrasound imaging system and method includes performing a gesture with a probe and detecting the gesture based on data from a motion sensing system includes at least one sensor selected from the group of an accelerometer, a gyro sensor and a magnetic sensor. However, US2014/0128739 A1 provide a solution to solve the power-consumption issue of ultrasound system and is silent about the above mentioned issue of PTX determination.

SUMMARY OF THE INVENTION

[0007] Therefore, it would be advantageous to provide an improved ultrasound system and method for sequentially performing automatic detection on different portions of a subject.

[0008] According to a first aspect of the present invention, there is proposed an ultrasound system for sequentially performing a predetermined procedure for each of at least one region of interest, comprising:

[0009] an ultrasound probe configured to transmit a first ultrasound signal towards a region of interest and receive echo signals from the region of interest;

[0010] a motion sensor configured to detect a motion of the ultrasound probe and generate a motion signal for indicating the motion of the ultrasound probe; and

[0011] a processor configured to perform a predetermined procedure for a region of interest on the basis of the echo signals received from the region of interest if the motion signal indicates that the ultrasound probe is stationary.

[0012] The whole PTX determination process according to the clinical protocol may seem to be very complex due to the multiple determination processes on multiple portions of the chest. However, inventors of the present invention recognized that the operator will operate in a repeated stop-and-go mode (i.e. the operator will move the ultrasound probe to a portion of the subject, stop for a certain period on the portion and then go to the next portion) to transfer among different portions, because there is a predefined order according to the clinical protocol for all the operators to follow. The ultrasound probe will be placed on the subject by the operator without any movement, when the operator believes that the probe is ready for collecting ultrasound data for the ultrasound system to perform a predetermined procedure, such as PTX check. That is to say, the ultrasound probe will be stationary when it has been placed on the region of interest, such as a portion of the chest, by the operator and is ready for obtaining ultrasound data for check.

[0013] The motion sensor will monitor the motion of the ultrasound probe and provides motion signal indicating the motion of the probe. When the motion signal indicates that ultrasound probe is stationary, the processor will be triggered to perform a predetermined procedure, such as PTX check, on the region of interest immediately. There will be no extra time delay because the ultrasound system does not require the operator to do any extra operations to control the system to start the predetermined procedure. There is no need to place any extra devices on the region of interest, the whole system is easy to be implemented and cost effective. Furthermore, the accuracy of the solution will be good as long as the operator has been trained to follow the clinical

protocol to sequentially perform the predetermined procedure for each of the at least one region of interest.

[0014] In an embodiment of the ultrasound system according to the present invention, the ultrasound probe is configured to start transmitting the first ultrasound signal if the motion signal indicates that the ultrasound probe is stationary. With this ultrasound system, the ultrasound probe is activated to start transmitting the first ultrasound signal when the ultrasound probe is detected to be stationary. The ultrasound probe is not activated when the ultrasound probe is detected to be not stationary, which saves energy and reduces ultrasound exposure.

[0015] In another embodiment of the ultrasound system according to the present invention, the ultrasound probe is configured to transmit a second ultrasound signal prior to transmitting the first ultrasound signal. This feature enables the ultrasound system to transmit the second ultrasound signal when the ultrasound probe is indicated to be not stationary. This feature allows the user access to ultrasound signals all the time. Consequently, the ultrasound signals are enabled to be visualized by the user all the time.

[0016] In an embodiment of the ultrasound system according to the present invention, the processor is further configured to generate an indication indicative of completion of the predetermined procedure. The processor enables to generate the indication timely after the predetermined procedure has been completed. The indicator indicating the condition enables providing information timely to the user. The user may move the ultrasound probe to the next region of interest in response to the indication of the indicator so as to minimize the required time spent at each region of interest.

[0017] In an embodiment of the ultrasound system according to the present invention, the ultrasound system further comprises a user interface configured to present the indication. This feature allows presenting the indication to the operator, so that the operator is aware of the completion of the predetermined procedure at the region of interest. For certain applications, the time required for performing the predetermined procedure may vary at different regions of interest. This feature allows presenting the user with timely information about the completion of the predetermined procedure at a region of interest. The user may move the ultrasound probe to the next region of interest in response to the indication so as to minimize the required time spent at each region of interest.

[0018] In an embodiment of the ultrasound system according to the present invention, the predetermined procedure for a region of interest comprises a procedure for extracting features of the region of interest from the echo signals received from the region of interest. This feature enables the ultrasound system to extract features of the region of interest automatically.

[0019] In an embodiment of the ultrasound system according to the present invention, the predetermined procedure for a region of interest comprises a procedure for detecting the presence of a pneumothorax on the basis of the echo signals received from the region of interest. This feature enables the ultrasound system to detect a pneumothorax in the region of interest automatically.

[0020] In an embodiment of the ultrasound system according to the present invention, the ultrasound system further comprises a reporting module, the processor is configured to deliver a result of the predetermined procedure for a region of interest, the reporting module is configured to identify a

current region of interest of the at least one region of interest in accordance with a predetermined order of the at least one region of interest and record a result delivered by the processor as a result for the current region of interest, the at least one region of interest comprising a plurality of regions of interest. The feature applies for a plurality of regions of interest. In this way, the result of each region of interest can be recorded in sequence automatically and no extra action by the operator is required. When there are lots of regions to be checked for a certain operation, such as PTX check, the time for recording the check result of each region will be greatly reduced. The whole workflow is simple for the operator to operate, and the check result can be well recorded without any error as long as the operator does the check in the right order according to the clinical protocol.

[0021] In an embodiment of the ultrasound system according to the present invention, the ultrasound system further comprises the user interface configured to visualize the results recorded by the reporting module. This feature allows visualizing the results recorded to the user.

[0022] In an embodiment of the ultrasound system according to the present invention, the ultrasound system further comprises the user interface for receiving a user input for going back, and a go-back module configured to identify the current region of interest on the basis of the recorded results and the user input. In this way, the operator can control the check process if the operator finds something not good enough or wrong.

[0023] In an embodiment of the ultrasound system according to the present invention, the ultrasound system further comprises a position verification module configured to calculate a ratio between the size of the ultrasound acoustic shadow and the total area of a region of interest from the echo signals received from the region of interest and generate a position indicator by comparing the ratio with a predetermined threshold. Optionally, the position indicator provides information on whether the ultrasound probe is placed properly on this region of interest or needs to be placed on another region of interest.

[0024] In an embodiment of the ultrasound system according to the present invention, the motion detector is an accelerometer. With the accelerometer as the motion sensor, high accuracy measurements can be obtained.

[0025] According to a second aspect of the present invention, an ultrasound method is provided, comprising the steps of:

[0026] transmitting a first ultrasound signal towards a region of interest and receiving echo signals from the region of interest;

[0027] detecting a motion of an ultrasound probe and generating a motion signal for indicating the motion of the ultrasound probe; and

[0028] performing a predetermined procedure for a region of interest on the basis of the received echo signals received from the region of interest if the motion signal indicates that the ultrasound probe is stationary.

[0029] In an embodiment of the ultrasound method according to the present invention, the ultrasound method further comprises a step of starting to transmit the first ultrasound signals if the motion signal indicates that the ultrasound probe is stationary.

[0030] In an embodiment of the ultrasound system according to the present invention, the ultrasound system further

comprises a step of transmitting a second ultrasound signal prior to transmitting the first ultrasound signal.

[0031] Detailed explanations and other aspects of the invention will be given below.

BRIEF DESCRIPTION OF THE DRAWINGS

[0032] Particular aspects of the invention will now be explained with reference to the embodiments described hereinafter and considered in connection with the accompanying drawings, in which identical parts or sub-steps are designated in the same manner:

[0033] FIG. 1 schematically depicts a diagram for a system according to an embodiment of the present invention;

[0034] FIG. 2 illustrates an example of an ultrasound probe according to an embodiment of the present invention;

[0035] FIG. 3 illustrates an example of an ultrasound signal according to an embodiment of the present invention;

[0036] FIG. 4 illustrates another example of an ultrasound signal according to an embodiment of the present invention;

[0037] FIG. 5 illustrates a flowchart of a PTX detection method according to an embodiment of the present invention;

[0038] FIG. 6 illustrates an example of a plurality of regions of interest according to an embodiment of the invention;

[0039] FIG. 7 illustrates an example of sequential results recorded according to an embodiment of the present invention;

[0040] FIG. 8 schematically depicts a flowchart of a method according to an embodiment of the present invention; and

[0041] FIG. 9 illustrates an example of performing predetermined procedures according to an embodiment of the present invention.

DETAILED DESCRIPTION OF THE INVENTION

[0042] The present invention will be described with respect to particular embodiments and with reference to the drawings, but the invention is not limited thereto but only by the claims. The drawings described are only schematic and are non-limiting. In the drawings, the size of some of the elements may be exaggerated and not drawn to scale for illustrative purposes.

[0043] FIG. 1 depicts a schematic diagram of a system 100 for sequentially performing a predetermined procedure for each of at least one region of interest, according to the present invention.

[0044] The ultrasound system 100 comprises an ultrasound probe 101 configured to transmit a first ultrasound signal SG1 towards a region of interest and receive echo signals from the region of interest. The ultrasound system 100 also comprises a motion sensor 102 configured to detect a motion of the ultrasound probe 101 and generate a motion signal MS for indicating the motion of the ultrasound probe 101. The ultrasound system 100 further comprises a processor 103 configured to perform a predetermined procedure for a region of interest on the basis of the echo signals received from the region of interest if the motion signal MS indicates that the ultrasound probe 101 is stationary.

[0045] FIG. 2 illustrates an example of the ultrasound probe 101 according to an embodiment of the present invention. The ultrasound probe 101 transmits a first ultra-

sound signal SG1 towards a region of interest ROI. The region of interest ROI is exposed to the first ultrasound signal SG1. When the region of interest ROI reflects part of the first ultrasound signal SG1 back, the first ultrasound signal SG1's echo signal EC received from the region of interest ROI is formed. The ultrasound probe 101 receives the echo signal EC relating to the first ultrasound signal SG1 from the region of interest ROI. Therefore, the echo signal EC contains information of the region of interest ROI.

[0046] The motion sensor 102 monitors the motion of the ultrasound probe 101 and generates a motion signal MS to indicate the motion of the ultrasound probe 101. For example, accelerometers are known devices to be used as the motion sensor 102. An accelerometer may be placed on the ultrasound probe 101 to measure acceleration data of the ultrasound probe 101. Thus, accurate real-time velocity of the accelerometer can be derived on the basis of the measured data. Hence, the motion status of the ultrasound probe 101 is derived accordingly.

[0047] Gyroscopes are also known devices. They are useful for measuring or maintaining orientation, and they may be used together with the accelerometer to determine motion in 6 dimensions. There are other known devices to detect motion, such as barometer, cameras, and GPS sensor, etc. The embodiments of the motion sensor 102 are not limited to those mentioned above.

[0048] Whether the ultrasound probe 101 is stationary can be determined in many ways.

[0049] In an embodiment, it may be determined that the ultrasound probe 101 is stationary if the ultrasound probe 101's velocity derived by the motion sensor 102 is less than the minimum value which can be measured by the motion sensor 102. The minimum value of the measured data depends on the motion sensor 102's accuracy. For example, a certain type of motion sensor can only measure velocity not less than 0.0005 cm/s.

[0050] In another embodiment, there will be a maximum velocity threshold for the ultrasound probe 101 to complete the predetermined procedure, and the maximum velocity threshold may be different for different types of detection. People skilled in ultrasound detection will think that the maximum velocity threshold is small enough for determining whether the ultrasound probe 101 is stationary. It may be determined that the ultrasound probe 101 is stationary if the ultrasound probe 101's velocity derived by the motion sensor 102 is below the maximum velocity threshold. The maximum velocity threshold may be equal or larger than the minimum value which can be measured by the motion sensor 102. For example, the maximum velocity threshold is 0.0009 cm/s when the motion sensor 102 can only measure velocity not less than 0.0005 cm/s.

[0051] The motion of the ultrasound probe 101 is monitored by the motion sensor 102. When the motion sensor 102 detects that the motion of the ultrasound probe 101 is stationary as described above, the motion sensor 102 generates a motion signal MS to indicate the stationary state of the ultrasound probe 101. Then, processor 103 starts to perform a predetermined procedure for a region of interest on the basis of the echo signals received from the region of interest immediately in response to the motion signal.

[0052] FIG. 3 illustrates an example of an ultrasound signal according to an embodiment of the present invention. In an embodiment of the invention, the ultrasound probe 101

is configured to start transmitting the first ultrasound signal SG1 if the motion signal MS indicates that the ultrasound probe 101 is stationary.

[0053] In an embodiment, an accelerometer is used to detect the motion of the ultrasound probe 101, and the motion signal MS is generated as illustrated in FIG. 3. Within the motion signal MS, there are stationary periods SP with low amplitude. When the velocity value derived from the amplitude of the stationary periods SP is less than the minimum value which can be measured by the motion sensor 102, for example, 0.0005 cm/s, the stationary periods SP indicate the stationary state of the ultrasound probe 101.

[0054] As illustrated in FIG. 3, when the motion signal MS generated from the motion sensor 102 indicates the stationary state of the ultrasound probe 101, the ultrasound probe 101 starts to transmit the first ultrasound signal SG1. The first ultrasound signal SG1 may be a sequence of ultrasound data frames. For example, the ultrasound probe 101 is activated coincidentally with the period when the motion signal MS indicates that the ultrasound probe 101 is stationary. The ultrasound probe 101 starts to transmit the first ultrasound signal SG1 when the ultrasound probe 101 is activated, i.e., when the ultrasound probe 101 is stationary.

[0055] FIG. 4 illustrates another example of an ultrasound signal according to an embodiment of the present invention. In another embodiment, the ultrasound probe 101 is configured to transmit a second ultrasound signal SG2 prior to transmitting the first ultrasound signal SG1. In this embodiment, as shown in FIG. 4, the ultrasound probe 101 transmits ultrasound signals continuously. When the motion sensor 102 detects that the ultrasound probe 101 is not stationary, the ultrasound probe 101 starts to transmit the second ultrasound signal SG2. The second ultrasound signal SG2 may be a sequence of ultrasound data frames as illustrated in FIG. 4. When the motion signal indicates that ultrasound probe 101 is stationary, the ultrasound probe 101 starts to transmit the first ultrasound signal SG1 to the region of interest.

[0056] The first ultrasound signal SG1 and the second ultrasound signal SG2 are synchronized with the motion signal MS by using the same time reference system. The first ultrasound signal SG1 and the second ultrasound signal SG2 may comprise ultrasound data frames generated under many modes, such as B-mode, Doppler mode.

[0057] In another embodiment, the processor 103 is further configured to generate an indication IDA indicative of completion of the predetermined procedure.

[0058] As illustrated in FIG. 3 and FIG. 4, the completion of the predetermined procedure is denoted as E0. When the predetermined procedure is completed for the region of interest, the processor 103 generates an indication immediately.

[0059] As illustrated in FIG. 1, in another embodiment, the ultrasound image system 100 may further comprise a user interface 107 configured to present the indication IDA.

[0060] The user interface 107 aims to present an indication IDA to the operator in order to guide the operator for the next step. For example, the operator is guided to move the ultrasound probe 101 to the next region of interest. The indication IDA presented by the user interface 107 may be visible or audible to the operator. One example is a light indicator, which uses different colours of the light to indicate different types of feedback signals. Another example is an icon on a display, which visualizes the statuses to represent

different types of feedback signals. An alternative example is a voice reminder, which provides audio instructions to guide the operator based on the different types of feedback signals. The embodiments of the user interface 107 are not limited to the examples mentioned above.

[0061] In another embodiment of the system 100, the predetermined procedure for a region of interest comprises a procedure for extracting features of the region of interest from the echo signals received from the region of interest.

[0062] In another embodiment of the system 100, the predetermined procedure for a region of interest comprises a procedure for detecting the presence of a pneumothorax on the basis of the echo signals received from the region of interest.

[0063] Ultrasound imaging is widely used for pneumothorax (PTX) detection. Four features have been described for PTX detection: lung sliding, B-lines, lung pulse and lung point.

[0064] FIG. 5 illustrates a flowchart of a PTX detection method according to an embodiment of the present invention. As illustrated in FIG. 5, the step of detection of the presence of lung sliding S1, the step of detection of the presence of lung pulse S2, or the step of detection of the presence of B-line S3 are performed. If one of the presence of lung sliding, lung pulse or B-line is detected, it means there is no PTX at this portion of the chest. The indication IDA indicating completion of the PTX detection is generated. The indicator 107 indicates accordingly to the operator. In this scenario, the indication to the operator is to move the ultrasound probe 101 to the next portion of the chest immediately after any one of the presence of lung sliding, lung pulse or B-line is detected.

[0065] When the presence of none of lung sliding, lung pulse or B-line is detected, the step of detection of the presence of lung point S4 is to be further performed by means of the algorithm, as illustrated in FIG. 5. In sequence, the indication IDA indicating completion of a PTX detection is generated. The user interface 107 accordingly presents the indication IDA to the operator. In this scenario, the indication to the operator is to move the ultrasound probe 101 to the next portion of the chest immediately after the lung point is detected.

[0066] At different portions of the chest, the time required for PTX detection may be different. A portion of the chest where PTX is detected normally takes up more time than a PTX-free portion of the chest. The decision of ruling out PTX may be made quickly as long as a detection of one of the features is absent, for example, lung sliding, lung-pulse, or B-lines as illustrated in FIG. 5. There is no need to acquire ultrasound data at each portion of the chest for at least one full breathing cycle to reach a decision about absence of PTX, which results in a saving of time at the portion the chest. Thus, by means of the user interface 107, the operator is able to move the ultrasound probe 101 to the next portion of the chest in response to the indication IDA presented by the user interface 107, thereby spending less time at each portion of the chest.

[0067] As illustrated in FIG. 1, in another embodiment, the ultrasound system 100 may further comprise a reporting module 108, the processor 103 is configured to deliver a result of the predetermined procedure for a region of interest, the reporting module 108 is configured to identify a current region of interest of the at least one region of interest in accordance with a predetermined order of the at least one

region of interest and record a result delivered by the processor **103** as a result for the current region of interest, the at least one region of interest comprising a plurality of regions of interest.

[0068] FIG. 6 illustrates an example of a plurality of regions of interest according to an embodiment of the invention. The ultrasound probe **101** is required to be placed on the plurality of regions of interest according to the predefined order of the clinical protocol. The predefined order may be shown by the user interface **107** and will be followed by all the operators. Referring to FIG. 6, the plurality of region of interest are a plurality of regions separated by lines along horizontal and vertical directions. The numbers shown in FIG. 6 indicate the order in which the ultrasound probe **101** is to be placed on the plurality of regions of interest, which is the predefined order. For each region of interest, there is a corresponding order in the sequence of the plurality of regions of interest.

[0069] The operator sequentially place the ultrasound probe **101** on the plurality of regions of interest and the processor **103** sequentially performs the predetermined procedure for the plurality of regions of interest. The reporting module **103** will identify the current region of interest as the first region of the plurality regions of interest when the ultrasound system **100** starts checking a certain subject and it is the first time that the motion signal MS generated by the motion sensor **102** indicates that the ultrasound probe **101** is stationary. Similarly, the reporting module **103** will identify the current region of interest as the second region of the plurality regions of interest when it is the second time that the motion signal MS generated by the motion sensor **102** indicates that the ultrasound probe **101** is stationary. Similarly, the reporting module **103** will identify the current region of interest as the nth region of the plurality regions of interest when it is the nth time that the motion signal MS generated by the motion sensor **102** indicates that the ultrasound probe **101** is stationary. In this way, the sequence of each region of interest among the plurality of region of interest can be identified and then the corresponding result of each region of interest can be recorded in association with each region of interest. FIG. 7 illustrates an example of sequential results recorded according to an embodiment of the present invention. For a region of interest ROI_i of the plurality of regions of interest, a corresponding result R_i is delivered, as illustrated in the upper part of FIG. 7. Moreover, there is a specific order number associated with the region of interest ROI_i derived from the predefined order, which is 1 in this example, as illustrated in the lower part of FIG. 7. The reporting module **108** identifies the current region of interest ROI_i from the plurality of regions of interest as the first region of interest. Consequently, the result R_i is associated with the identified current region of interest ROI_i.

[0070] As illustrated in FIG. 1, in another embodiment, the ultrasound system **100** may further comprise the user interface **107** configured to visualize the results recorded by the reporting module **108**.

[0071] The results recorded by the reporting module **108** may be visualized on the user interface **107** directly. Alternatively, the results may be mapped on pre-acquired information and visualized together with the pre-acquired information. The pre-acquired information may be anatomy

information of the plurality of regions of interest, such as CT images, MR images, or anatomy models of the plurality of regions of interest.

[0072] As illustrated in FIG. 1, in another embodiment, the ultrasound system **100** further comprises the user interface **107** for receiving a user input to go back and a go-back module **105** configured to identify the current region of interest on the basis of the recorded results and the user input.

[0073] The user interface **107** enables the user to give an input to go back, for example, when the user feels the operation is not done properly or the operation is not satisfactory for a region of interest, the user may give an input to go back, i.e., not record the result for the region of interest. Based on the user input to go back, the go-back module **105** identifies the current region of interest and records the results.

[0074] For example, in FIG. 7, the results of the predetermined procedure for the plurality of regions of interest are recorded sequentially. The predetermined procedure for a region of interest ROI_p is completed, the corresponding order of which is k-1 on the basis of the predefined order. Then, the ultrasound probe **101** is moved to the next region of interest according to the predefined order, whose order is k. Referring to FIG. 7, a region of interest ROI_q is the current region of interest. If the go-back module **105** receives the user input to go back at this moment, then the region of interest ROI_p becomes the current region of interest. Accordingly the predetermined procedure is started all over again for the current ROI, such as ROI_p in this embodiment.

[0075] In another embodiment, the ultrasound system **100** may further comprise a position verification module **110** configured to calculate a ratio between the size of the ultrasound acoustic shadow and the total area of a region of interest from the echo signals received from the region of interest and generate a position indicator by comparing the ratio with a predetermined threshold.

[0076] The embodiment is shown in FIG. 1. When the ultrasound probe **101** is placed at a region of interest, based on the comparison of the ratio with the predetermined threshold, the position verification module **110** generates the position indicator showing whether the ultrasound probe **101** is placed properly. If the position indicator shows the ultrasound probe **101** is not placed properly, the operator needs to change the position of the ultrasound probe **101** until the position indicator shows that the ultrasound probe **101** is placed properly. Then the ultrasound probe **101**, the motion detector **102** and the processor **103** start operating.

[0077] The ultrasound acoustic shadow is formed when ultrasound signals are blocked by a portion of the living being, for example, a bone or bony structure. For example, when the ultrasound probe **101** is placed on the chest, the ultrasound signals generated by the ultrasound probe **101** are not able to pass through ribs. The ratio between the size of the ultrasound acoustic shadow and the total area of a region of interest indicates whether the ultrasound probe **101** is placed on the correct position. The larger is the ratio, the better is the position for placing the ultrasound probe **101**.

[0078] For example, there are dark areas under the ribs in acquired ultrasound images. Therefore, one embodiment is provided to calculate the ratio by using the acquired ultrasound images. In this embodiment, the ratio between the size of the ultrasound acoustic shadow and the total area of a

region of interest is represented by the ratio between the area of the ultrasound acoustic shadow and the total area of the ultrasound image frame. The width of an ultrasound image frame is the width of the ultrasound probe **101**, which can be measured directly. The depth of an ultrasound image frame is determined by the operator before the operation. Therefore, the total area of the ultrasound image frame is calculated by multiplying the width of the ultrasound image frame and the depth of the ultrasound image frame.

[0079] The area of the ultrasound acoustic shadow may be determined by applying a known image processing algorithm to the ultrasound image frame, for example, detecting the edge to identify the range of the ultrasound acoustic shadow and then calculate the area of the identified range.

[0080] The predetermined threshold is chosen in the range of $[1/4-1/3]$ based on experimental results. A ratio smaller than the predetermined threshold indicates that the ultrasound probe **101** is placed at a proper position. A ratio larger than the predetermined threshold indicates that the ultrasound probe **101** is not placed at a proper position.

[0081] In another embodiment of the system **100**, the motion sensor **102** is an accelerometer.

[0082] The accelerometer may be a 3-axis accelerometer, adapted to detect acceleration in any of three orthogonal directions. For example, a first axis of the accelerometer may be disposed in an x-direction, a second axis may be disposed in a y-direction, and a third axis may be disposed in a z-direction. By combining signals from each of the three axes, the accelerometer may be able to detect accelerations in any three-dimensional direction. By integrating accelerations occurring over a period of time, the processor may generate an accurate real-time velocity of the accelerometer on the basis of data from the accelerometer.

[0083] FIG. **8** schematically depicts a flowchart of a method according to the present invention.

[0084] An ultrasound method **200** for sequentially performing a predetermined procedure for each of at least one region of interest, comprises a step of transmitting **201** a first ultrasound signal SG1 towards a region of interest and receiving echo signals from the region of interest. The ultrasound method **200** also comprises a step of detecting **202** a motion of an ultrasound probe **101** and generating a motion signal MS for indicating the motion of the ultrasound probe **101**. The ultrasound method **200** also comprises a step of performing **203** a predetermined procedure for a region of interest on the basis of the echo signals received from the region of interest if the motion signal MS indicates that the ultrasound probe **101** is stationary.

[0085] In an embodiment, the ultrasound method **200** may further comprise a step of starting to transmit the first ultrasound signals SG1 if the motion signal MS indicates that the ultrasound probe **101** is stationary.

[0086] In an embodiment, the ultrasound method **200** may further comprise a step of transmitting a second ultrasound signals SG2 prior to transmitting the first ultrasound signal SG1.

[0087] While the invention has been illustrated and described in detail in the drawings and foregoing description, such illustration and description are to be considered illustrative or exemplary and not restrictive. The invention is not limited to the disclosed embodiments. Other variations to the disclosed embodiments can be understood and

effected by those skilled in the art in practicing a claimed invention, from a study of the drawings, the disclosure, and the dependent claims.

[0088] In the claims, the word “comprising” does not exclude other elements or steps, and the indefinite article “a” or “an” does not exclude a plurality. A single processor or other unit may fulfill the functions of several items re-cited in the claims. The mere fact that certain measures are re-cited in mutually different dependent claims does not indicate that a combination of these measures cannot be used to advantage. Any reference signs in the claims should not be construed as limiting the scope.

1. An ultrasound system for sequentially performing a predetermined procedure for each of at least one region of interest, comprising:

an ultrasound probe configured to transmit a first ultrasound signal towards a region of interest and receive echo signals from the region of interest;

a motion sensor configured to detect a motion of the ultrasound probe and generate a motion signal (MS) for indicating the motion of the ultrasound probe; and

a processor configured to perform a predetermined procedure for a region of interest on the basis of the echo signals received from the region of interest if the motion signal (MS) indicates that the ultrasound probe is stationary.

2. An ultrasound system as claimed in claim 1, wherein the ultrasound probe is configured to start transmitting the first ultrasound signal (SG1) if the motion signal (MS) indicates that the ultrasound probe is stationary.

3. An ultrasound system as claimed in claim 2, wherein the ultrasound probe is configured to transmit a second ultrasound signal (SG2) prior to transmitting the first ultrasound signal (SG1).

4. An ultrasound system as claimed in claim 1, wherein the processor is further configured to generate an indication (IDA) indicative of completion of the predetermined procedure.

5. An ultrasound system as claimed in claim 4, further comprising:

a user interface configured to present the indication (IDA).

6. An ultrasound system as claimed in claim 1, wherein the predetermined procedure for a region of interest comprises a procedure for extracting features of the region of interest from the echo signals received from the region of interest.

7. An ultrasound system as claimed in claim 6, wherein the predetermined procedure for a region of interest comprises a procedure for detecting a pneumothorax on the basis of the echo signals received from the region of interest.

8. An ultrasound system as claimed in claim 1, further comprising a reporting module, wherein the processor is configured to deliver a result of the predetermined procedure for a region of interest, wherein the reporting module is configured to identify a current region of interest of the at least one region of interest in accordance with a predetermined order of the at least one region of interest and record a result delivered by the processor as a result for the current region of interest, wherein the at least one region of interest comprises a plurality of region of interests.

9. An ultrasound system as claimed in claim 8, further comprising:

the user interface configured to visualize the results recorded by the reporting module.

10. An ultrasound system as claimed in claim **8**, further comprising:

the user interface for receiving a user input to go back; and

a go-back module configured to identify the current region of interest on the basis of the recorded results and the user input.

11. An ultrasound system as claimed in claim **1**, further comprising:

a position verification module configured to calculate a ratio between the size of the ultrasound acoustic shadow and the total area of a region of interest from the echo signals received from the region of interest and generate a position indicator by comparing the ratio with a predetermined threshold.

12. An ultrasound system as claimed in claim **1**, wherein the motion sensor is an accelerometer.

13. An ultrasound method for sequentially performing a predetermined procedure for each of at least one region of interest, comprising the steps of :

transmitting a first ultrasound signal (SG1) towards a region of interest and receiving echo signals from the region of interest;

detecting a motion of an ultrasound probe and generate a motion signal (MS) for indicating the motion of the ultrasound probe; and

performing a predetermined procedure for a region of interest on the basis of the echo signals received from the region of interest if the motion signal (MS) indicates that the ultrasound probe is stationary.

14. An ultrasound method as claimed in claim **13**, further comprising a step of:

starting to transmit the first ultrasound signal (SG1) if the motion signal (MS) indicates that the ultrasound probe is stationary.

15. An ultrasound method as claimed in claim **14**, further comprising a step of

transmitting a second ultrasound signal (SG2) prior to transmitting the first ultrasound signal (SG1).

* * * * *

专利名称(译)	超声系统和方法		
公开(公告)号	US20190150889A1	公开(公告)日	2019-05-23
申请号	US16/066723	申请日	2016-12-19
[标]申请(专利权)人(译)	皇家飞利浦电子股份有限公司		
申请(专利权)人(译)	皇家飞利浦N.V.		
当前申请(专利权)人(译)	皇家飞利浦N.V.		
[标]发明人	XU JINGPING RAJU BALASUNDAR IYYAVU WANG SHOUGANG POLAND MCKEE DUNN GADES ANTHONY M		
发明人	XU, JINGPING RAJU, BALASUNDAR IYYAVU WANG, SHOUGANG POLAND, MCKEE DUNN GADES, ANTHONY M.		
IPC分类号	A61B8/00 A61B8/08		
CPC分类号	A61B8/4281 A61B8/4254 A61B8/4483 A61B8/467 A61B8/5223 A61B8/08 A61B8/461 A61B8/488 A61B8/5207 A61B8/54 G16H50/30		
优先权	PCT/CN2015/099880 2015-12-30 WO 2016159416 2016-03-09 EP		
外部链接	Espacenet USPTO		

摘要(译)

本发明涉及一种超声系统 (100) , 用于对至少一个感兴趣区域中的每一个依次执行预定程序。超声系统 (100) 包括超声探头 (101) , 其被配置为朝向感兴趣的区域发送第一超声信号 (SG 1) 。并从感兴趣的区域接收回波信号。超声系统 (100) 还包括运动传感器 (102) , 其被配置为检测超声探头的运动 (101) 并且生成运动信号 (MS) , 用于指示超声探头的运动 (101) 。超声系统 (100) 还包括处理器 (103) , 其被配置为基于从区域接收的回波信号对感兴趣区域执行预定程序。如果运动信号 (MS) 指示超声探头 (101) 是静止的, 则感兴趣。本发明还涉及相应的超声方法。

