



US009655591B2

(12) **United States Patent**
Chaggares et al.

(10) **Patent No.:** **US 9,655,591 B2**
(45) **Date of Patent:** ***May 23, 2017**

(54) **ULTRASONIC PROBE AND ALIGNED
NEEDLE GUIDE SYSTEM**

(71) Applicant: **FUJIFILM SonoSite, Inc.**, Bothell,
WA (US)

(72) Inventors: **N. Chris Chaggares**, Whitby (CA);
Eric Michael Rieder, Georgetown
(CA)

(73) Assignee: **FUJIFILM SonoSite, Inc.**, Bothell,
WA (US)

(*) Notice: Subject to any disclaimer, the term of this
patent is extended or adjusted under 35
U.S.C. 154(b) by 0 days.

This patent is subject to a terminal dis-
claimer.

(21) Appl. No.: **14/746,633**

(22) Filed: **Jun. 22, 2015**

(65) **Prior Publication Data**

US 2016/0038118 A1 Feb. 11, 2016

Related U.S. Application Data

(63) Continuation of application No. 13/545,352, filed on
Jul. 10, 2012, now Pat. No. 9,113,825.

(51) **Int. Cl.**

A61B 8/00 (2006.01)

A61B 8/12 (2006.01)

(Continued)

(52) **U.S. Cl.**

CPC **A61B 8/4455** (2013.01); **A61B 8/0841**
(2013.01); **A61B 8/12** (2013.01);

(Continued)

(58) **Field of Classification Search**

CPC . A61B 10/02; A61B 10/0241; A61B 10/0275;
A61B 17/3403; A61B 2010/045;

(Continued)

(56) **References Cited**

U.S. PATENT DOCUMENTS

5,235,987 A 8/1993 Wolfe
5,437,283 A 8/1995 Ranalletta et al.

(Continued)

FOREIGN PATENT DOCUMENTS

EP 0955010 A 11/1999
JP 58-7230 1/1983

(Continued)

OTHER PUBLICATIONS

European Patent Office, Extended European Search Report, EP
Patent Application 13816371.2, mailed Feb. 9, 2016, 10 pages.

(Continued)

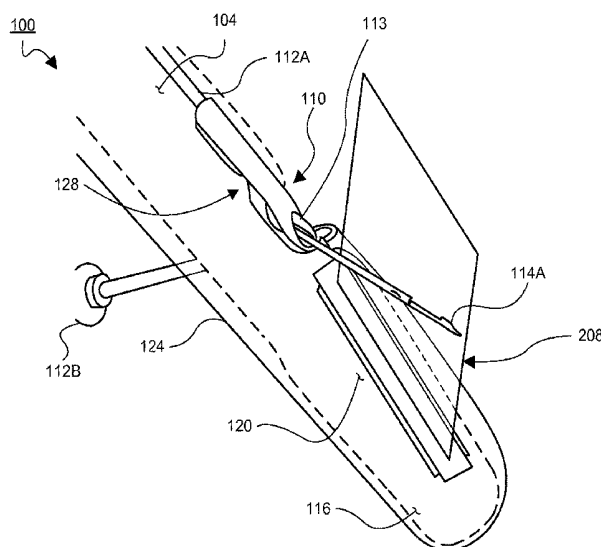
Primary Examiner — Michael Rozanski

(74) *Attorney, Agent, or Firm* — Perkins Coie LLP

(57) **ABSTRACT**

A side-fire ultrasonic probe includes an alignment feature that, when used to connect the probe with a needle guide for intra-cavity medical procedures, enables alignment of a needle in an imaging plane of an ultrasonic transducer. The alignment feature is configured such that alignment of the needle within the imaging plane is accomplished when a protective sheath is disposed between the alignment feature and the needle guide. This configuration can be used with high frequency ultrasonic arrays having frequency distributions centered at about 20 MHz, and for medical procedures, such as biopsying organs or other bodily intra-cavity structures, and delivering intra-cavity therapies.

12 Claims, 3 Drawing Sheets



(51) **Int. Cl.**

A61B 10/02 (2006.01)
A61B 8/08 (2006.01)
A61B 17/34 (2006.01)
A61B 17/00 (2006.01)
A61B 10/04 (2006.01)

(52) **U.S. Cl.**

CPC *A61B 8/4422* (2013.01); *A61B 8/4494*
 (2013.01); *A61B 10/02* (2013.01); *A61B*
10/0241 (2013.01); *A61B 10/0275* (2013.01);
A61B 17/3403 (2013.01); *A61B 8/445*
 (2013.01); *A61B 8/4444* (2013.01); *A61B*
2010/045 (2013.01); *A61B 2017/00274*
 (2013.01); *A61B 2017/3413* (2013.01)

(58) **Field of Classification Search**

CPC .. *A61B 2017/00274*; *A61B 2017/3413*; *A61B*
8/0841; *A61B 8/12*; *A61B 8/4422*; *A61B*
8/4444; *A61B 8/445*; *A61B 8/4455*; *A61B*
8/4494

See application file for complete search history.

FOREIGN PATENT DOCUMENTS

JP	02071732 A	3/1990
JP	4-77908	7/1992
JP	09201360 A	8/1997
JP	10028687 A	2/1998
JP	2000201936 A	7/2000
JP	2001500026 A	1/2001
JP	2001120550 A	5/2001
JP	2003299654 A	10/2003
JP	2005034273 A	2/2005
JP	2006506128 A	2/2006
JP	2006212166 A	8/2006
JP	2007244415 A	9/2007
JP	2007289693 A	11/2007
JP	2008253647 A	10/2008
JP	2011505206 A	2/2011
WO	2007124265 A2	11/2007
WO	2007124265 A3	1/2008
WO	2014009810	1/2014

OTHER PUBLICATIONS

(56)

References Cited

U.S. PATENT DOCUMENTS

6,261,234 B1	7/2001	Lin
6,443,902 B1	9/2002	Sasady
7,691,066 B2	4/2010	Kosaku
7,750,536 B2	7/2010	Chaggares et al.
9,113,825 B2	8/2015	Chaggares et al.
2006/0184034 A1	8/2006	Haim et al.
2007/0129632 A1	6/2007	Voie et al.
2007/0232924 A1	10/2007	Karasawa et al.
2014/0018667 A1	1/2014	Chaggares et al.

Krieger, Axel et al. "Design of a Novel MRI Compatible Manipulator for Image Guided Prostate Interventions." IEEE Transactions on Biomedical Engineering, vol. 52, No. 2, Feb. 2005, pp. 306-313.
 Yacoub, Joseph H. et al. "Imaging-guided Prostate Biopsy: Conventional and Emerging Techniques." RadioGraphics 2012, vol. 32, No. 3, pp. 819-838.

International Searching Authority, International Search Report and Written Opinion; PCT Application PCT/IB2013/001979, mailed Jan. 22, 2014, 9 pages.

Japanese Patent Office, Official Action, JP Patent Application 2015-521082, mailed Aug. 8, 2016, 12 pages; with English translation.

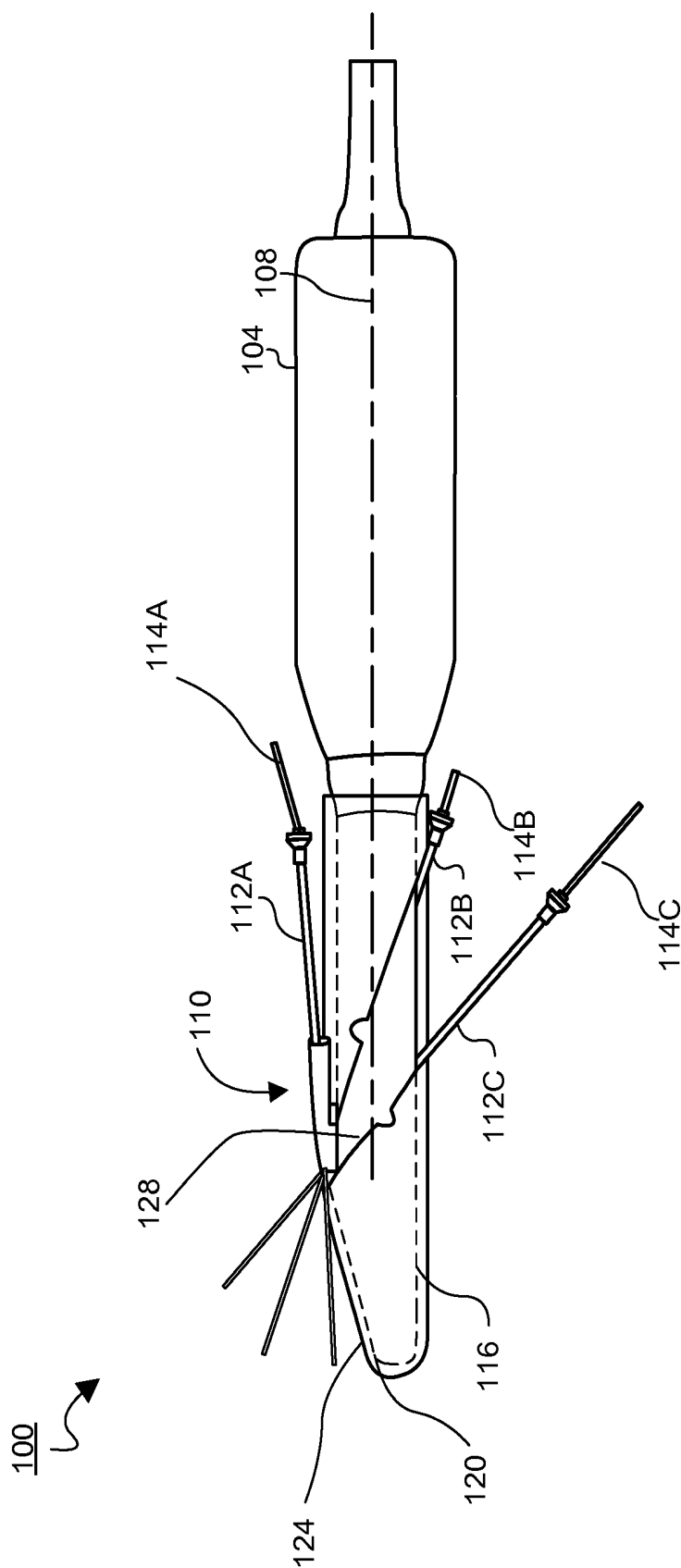


FIG. 1

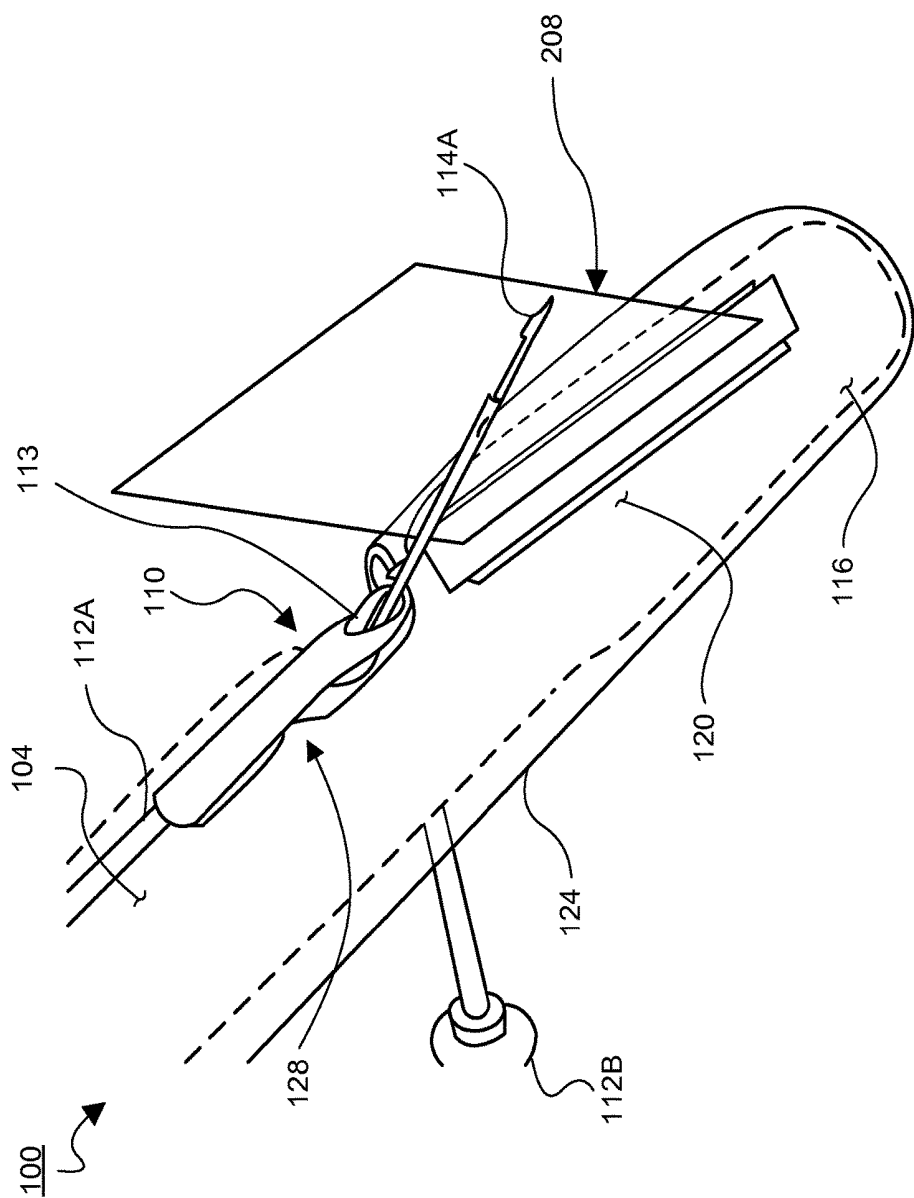


FIG. 2

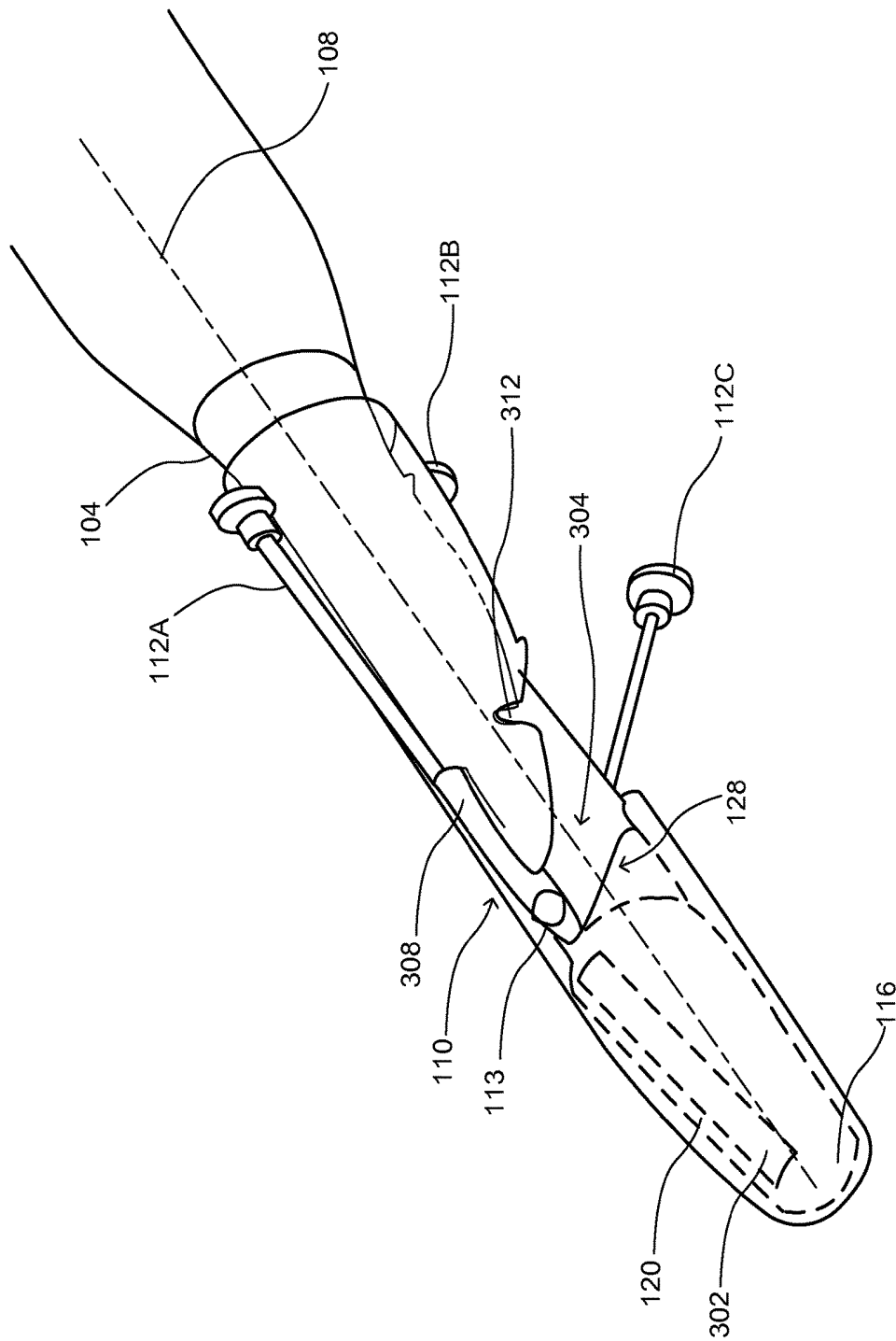


FIG. 3

1

ULTRASONIC PROBE AND ALIGNED NEEDLE GUIDE SYSTEM

CROSS-REFERENCE TO RELATED APPLICATIONS

This application is a continuation of U.S. patent application Ser. No. 13/545,352, filed Jul. 10, 2012, now U.S. Pat. No. 9,113,825, which is hereby incorporated by reference in its entirety.

BACKGROUND

The present disclosure relates generally to medical imaging and diagnostics, and more specifically to an ultrasonic probe and an aligned needle guide system.

Accessing organs and structures of the human body through body cavities is a standard medical technique. In some procedures, diagnostic tools are inserted into a body cavity to examine or biopsy an organ or other body structure. The information collected is then used for the detection and evaluation of a wide variety of medical conditions. In particular, ultrasonic devices are used to identify intra-cavity structures, such as a prostate, by transmitting and receiving ultrasonic waves. The received waves are transformed into an image of the intra-cavity structure, which can then be used to navigate a biopsy needle to a desired location within the image.

Ultrasonic transducers used in these medical applications are typically encased within an anatomically compatible housing to improve patient comfort during insertion into the patient. Ultrasonic transducer housings fall into one of two broad configuration types: “end-fire” and “side-fire.” The end-fire type transmits ultrasonic waves from a tip of the housing, whereas the side-fire type transmits from a side-wall of the housing. Regardless of the housing type, the ultrasonic image can be used to navigate a biopsy needle to an exterior surface of an intra-cavity bodily structure.

SUMMARY

In one embodiment, an ultrasonic probe of the present disclosure includes a cylindrical housing that includes a needle guide alignment feature on the surface of the housing. The alignment feature is used to connect a needle guide to the cylindrical housing and to align the needle guide such that a needle translated through the guide is translated in an imaging plane of the ultrasonic transducer. The alignment feature is configured such that the needle is aligned in the imaging plane even when a protective sheath is disposed between the housing and the needle guide. The protective sheath may facilitate sanitation, sterilization, and re-use of the probe.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 illustrates an example of an ultrasonic probe with an aligned needle guide, in an embodiment.

FIG. 2 is a perspective view of a tip of an ultrasonic probe, wherein the probe is encased in a protective sheath and, using a needle guide, a needle is aligned in an imaging plane produced by an ultrasonic transducer, the alignment facilitated by an alignment feature disposed on the housing, in an embodiment.

FIG. 3 is perspective view of an ultrasonic probe covered by a protective sheath and an attached needle guide aligned with the probe, in an embodiment.

2

The figures depict various embodiments of the present invention for purposes of illustration only. One skilled in the art will readily recognize from the following discussion that alternative embodiments of the structures and methods illustrated herein may be employed without departing from the principles of the invention described herein.

DETAILED DESCRIPTION

10 Overview

Embodiments described herein include a side-fire ultrasonic probe with an alignment feature that, when used to connect the probe to a needle guide for intra-cavity medical procedures (e.g., biopsying organs or other bodily intra-cavity structures, delivering intra-cavity therapies), facilitates alignment of one or more needles translated through the needle guide with an imaging plane of an ultrasonic transducer. The alignment feature is configured such that alignment of a needle within the imaging plane is accomplished even when a protective sheath is disposed between the alignment feature and the needle guide.

By positioning the translated needles within the imaging plane of a side-fire type ultrasonic probe, an ultrasonic image can be used to image an advancing needle with respect to an intra-cavity structure of interest. This ability is particularly useful when the ultrasonic transducer has a frequency and/or resolution sufficient to image intra-structure or intra-organ features. Simultaneously imaging the structure of interest and the needle permits navigation of the needle to a specific intra-cavity structure within a human body, or, given sufficient resolution of the ultrasonic transducer, navigation of the needle to a specific location within the structure. This can then improve the diagnostic capability of the procedure or effectiveness of the therapy. Allowing for positioning of a needle oriented at different angles with respect to the probe enables access to a range of locations within the body or structure by the needles while reducing the manipulation of the probe. This can improve patient comfort during the procedure, as well as patient safety.

40 Ultrasonic Probe and Aligned Needle Assembly

FIG. 1 illustrates an embodiment of a side-fire ultrasonic probe assembly **100** having an alignment feature that enables alignment of a needle guide **110** such that needles (e.g., any of needles **114A-C**, “**114**” for brevity) translated through the guide are translated into an imaging plane produced by the ultrasonic transducer array. The imaging plane is defined by a pathway of ultrasonic waves produced by the ultrasonic transducer. The ultrasonic probe assembly **100** includes a cylindrical housing **104** having a longitudinal axis **108**, and a transducer housing **116** having an angled face **120**. The transducer housing **116** encloses an ultrasonic transducer array used for the production of ultrasonic waves, the reflections of which are transformed into images. A protective sheath **124**, disposed between the cylindrical housing **104** and the needle guide **110**, covers a portion of the cylindrical housing and the transducer housing **116**. The ultrasonic probe assembly **100** also includes a needle assembly alignment feature **128**, shown in more detail in FIGS. 2 and 3.

The cylindrical housing **104** of the ultrasonic probe assembly **100** has a number of uses including, but not limited to, enclosing wiring and/or electronic components used to operate the ultrasonic transducer, providing a structure with which to connect other elements of the assembly (e.g., the needle guide **110**), and providing a proximal end (i.e., a handle) used by an operator for manipulating the assembly. In this example, the cylindrical housing **104** has a

circular or elliptical cross-section that is ergonomically insertable into a body cavity, such as a rectum, to image, biopsy, and/or deliver a therapy to a body structure of interest, such as a prostate. While other embodiments of the cylindrical housing **104** are not limited to cylinders or circular or elliptical cross-sections, housings having points or edges may cause patient discomfort or damage sensitive tissue. The longitudinal axis **108** of the cylindrical housing **104** is parallel to the long axis of the cylindrical housing and is used as a convenient reference when describing other features of the embodiments.

The needle guide **110**, which includes individual guide channels **112A-C** (“**112**” collectively), into which one or more of the needles **114** can be inserted, is attached to the cylindrical housing **104** over the protective sheath **124** using the alignment feature **128**. The details of the needle guide **110** are described in more detail in the context of FIGS. **2** and **3**.

One needle of the needles **114** is used to biopsy intra-cavity structures of interest, such as a prostate (shown in FIG. **1** by an ellipse), by being translated through one channel **112** of the needle guide **110**, through port **113** (shown in FIGS. **2** and **3**), and into the ultrasonic imaging plane. The three channels **112** are oriented at different angles with respect to the horizontal axis **108** of the probe assembly **100** so that different locations within the body structure can be accessed by a needle **114** without moving the probe within the patient. Because both the needle (e.g., needle **114A**) and the structure of interest are in the imaging plane simultaneously, and therefore both imaged using reflected ultrasonic waves, the needle can be navigated to a specific location of interest. This location can be on the surface of the body structure or, provided that the ultrasonic transducer is capable of intra-structure resolution (typically achieved at high transducer frequencies of approximately 20 MHz), even within a specific body structure.

The transducer housing **116** is located at the distal end of the cylindrical housing **104**. The transducer housing **116** substantially surrounds the ultrasonic transducer used to produce ultrasonic waves. In this example, the transducer housing **116** is ergonomically shaped to improve patient comfort during insertion of the assembly **100** into a body cavity. This ergonomic shape can also improve patient comfort during operation of the assembly **100** for imaging and biopsying intra-cavity body structures.

In this example, because the ultrasonic transducer transmits ultrasonic waves through a sidewall of the cylindrical housing **104**, the design of the assembly **100** is sometimes referred to as a “side-fire” design. Other embodiments of the invention may be used with “end-fire” designs, in which the ultrasonic waves are transmitted from a terminal end of the transducer housing **116** (i.e., in a direction generally parallel to the longitudinal axis **108**).

The transducer housed by the transducer housing **116** may comprise an array of piezoelectric elements that produce ultrasonic waves when electrically actuated. In some examples, the transducer array can produce ultrasonic waves having a frequency distribution centered between approximately 1 MHz and 12 MHz. The resolution of images produced at these lower frequencies may be sufficient to discern the outline and/or outer surfaces of intra-cavity body structures. In other examples, the transducer array can produce ultrasonic waves having a frequency distribution centered at approximately 20 MHz and a 6 dB corner frequency of approximately 27 MHz. The resolution of images produced at these higher frequencies may be sufficient to image structures within the intra-cavity body struc-

tures (i.e., intra-organ resolution). This higher resolution and imaging facilitates navigation of the needles **114A-C** to locations within the body structure, which can then be biopsied. Also, because the interior of the organ or body structure can be imaged, this resolution can also help prevent accidental damage to the body structure.

The above description of the approximate center of the frequency distribution is important due to inconsistent description of transducer operating frequency in the art: while some artisans describe operating frequency by citing the center of the frequency distribution, other artisans describe operating frequency by citing the upper limit of the distribution.

The side-fire design of the transducer housing **116** includes the angled face **120**, which facilitates acoustic coupling between the transducer and the body structure to be imaged. By matching the angle of the angled face **120** to the shape of the body structure, the transducer and thus the ultrasonic waves used to image the body structure are brought proximate to a surface of the body structure without angling the assembly **100** as a whole. This improves the quality of the image and comfort of the patient by reducing the manipulation of the probe **100** needed to acquire an image. In some embodiments, the angled face **120** is angled about 13° to match a typical slope of a prostate surface. In other embodiments, the angled face **120** is angled at least 5°. In further embodiments, this angle can be varied depending on the natural angle (or range of natural angles) of the body structure surface to be imaged. In still further embodiments, the transducer housing **116** does not have an angled face, but rather is a standard side-fire design.

In the example shown, the protective sheath **124** covers the transducer housing **116**, and at least a portion of the cylindrical portion **104**. Acting as a barrier, the protective sheath **124** prevents body fluids or other substances from contaminating the assembly **100**. By limiting access of body fluids and contaminants to the interior and exterior of the assembly **100**, the protective sheath **124** facilitates sanitation, sterilization, and re-use of the assembly.

In some examples, the protective sheath **124** is designed to match the shape of the assembly **100**, including the cylindrical housing **104**, the transducer housing **116**, the angled face **120**, and the alignment feature **128**. In other examples, the protective sheath **124** is designed to match the shape of conventional ultrasonic probe assemblies and not is customized to match the shape of the assembly **100**. In some examples, the protective sheath **124** is made from a polymer, although other materials that permit the transmission and reception of ultrasonic waves can be used.

Needle Alignment

The alignment feature **128** is configured such that a **114** is aligned with and disposed in the imaging plane (shown in FIG. **2**) when the needle guide **110** is engaged with the alignment feature through the protective sheath **124** and the needle has been translated through one of the channels **112** of the needle guide and through the port **113** into the imaging plane. In some embodiments, the alignment feature **128** is a negative feature imprinted, molded, or embossed into the surface of cylindrical housing **104** and configured to mate with an approximately matching positive feature on the needle guide **110**. This negative profile enables the needle guide **110** to connect to the cylindrical housing **104**, enabling the imaging of a needle **114** during a procedure, as described above, while also maintaining an anatomically compatible profile. In other embodiments, the alignment feature **128** is a positive feature attached, connected, or integrated onto the

surface the cylindrical housing 104. In still other embodiments, the alignment feature 128 is a combination of positive and negative features.

In some examples, the alignment feature 128 is designed to connect the needle guide 110 to the cylindrical housing 104 and maintain alignment of the needles 114 in the ultrasonic imaging plane when the protective sheath 124 is disposed between the cylindrical housing and the needle assembly. In some embodiments of this example, the alignment feature 128 can be adjusted to accommodate thickness variations of the protective sheath 124, thereby maintaining alignment of the needle 114 in the imaging plane regardless of sheath thickness. In other examples, the alignment feature 128 is designed to maintain alignment between the needle 114 and the imaging plane without adjustment and regardless of the thickness of the protective sheath 124.

FIG. 2 illustrates the alignment of the needle 114A in the acoustic imaging plane of the ultrasonic probe assembly 100, as discussed above. This figure depicts a portion of the needle guide 110, the alignment feature 128, the needle 114A, and an acoustic imaging plane 208. As will be appreciated, the needle 114A is selected only for convenience. Embodiments of the present disclosure are applicable to the needles 114B and 114C, which can be translated through the corresponding needle guide channels 112 and emerge from port 113 at different angles with respect to the horizontal axis 108 of the probe 100 into the imaging plane 208. Also shown in FIG. 2 are portions of the cylindrical housing 104, the transducer housing 116, the angled face 120, and the protective sheath 124.

In the example shown, the cylindrical housing 104 and the transducer housing 116 are protected by the protective sheath 124. The needle guide 110 is disposed in the alignment feature 128, in this example a negative feature on the surface of the cylindrical housing 104, thereby compressing the protective sheath 124 into the alignment feature.

As shown, the needle guide 110, the needle 114A, the alignment feature 128, the protective sheath 124, and the transducer are configured such that the needle is disposed within the imaging plane 208 when extended distally through the needle guide 110. As mentioned above, this enables the needle 114A to be viewed during use and, in particular, enables the needle to be navigated to the body structure of interest. Furthermore, for examples of the ultrasonic probe assembly 100 using a transducer having frequencies centered at approximately 20 MHz, the needle 114A can be navigated to intra-organ features, thereby enabling precision biopsy or treatment of specific intra-organ areas.

In one aspect, this alignment of the needle 114A and the image plane 208 is accomplished by configuring the needle guide 110, a needle 114, and the alignment feature 128 such that the needle is positioned in the imaging plane 208 at a location in the imaging plane that is a function of how far the needle is translated. This alignment is further accomplished by controlling the dimensional tolerances of the various components to a total of approximately half of the width of the imaging plane 208. Controlling the total dimensional variation to only a portion of the width of the imaging plane permits some dimensional and/or alignment variation in the various components while still enabling the needle 114A to be translated into the imaging plane 208.

In one embodiment of the above example, ultrasonic transducers having a frequency distribution centered at about 20 MHz produce an imaging plane from approximately 300 microns to approximately 500 microns wide. By configuring the various components (e.g., the housing 104,

the alignment feature 128, the needle guide 110, and the protective sheath 124) described above, and controlling the combined dimensional variation of these components to approximately 250 microns, the needle 114A can be reliably imaged during and after its translation into the imaging plane 208.

In examples in which the diameter of the needle 114A is larger than the imaging plane 208 (e.g., a needle approximately 1000 microns in diameter used with an imaging plane approximately 500 microns wide), the entire diameter of the needle need not be in the imaging plane to image the needle and navigate it to a body structure location. Rather, a section that includes the needle point can be used to navigate the needle safely to, and into, the structure.

Needle Guide

FIG. 3 illustrates an ultrasonic probe 300 that includes an ultrasonic transducer 302, and the needle guide 110 attached to the cylindrical housing 104 over the protective sheath 124 using the alignment feature 128. In this example, the needle guide 110 includes the channels 112A-C, the port 113, a frame 304, a needle housing 308, and a positioning feature 312.

In this example, the three needles 114A-C are shown in each of the three channels 112A-C of the needle guide 110 to illustrate the different angles at which the channels are oriented with respect to the longitudinal axis 108 of the housing 104. This diversity of angles is used to increase the range of locations within the body accessible by the needles while minimizing the manipulation required of the assembly 100 needed to access these locations. Because the needles 114 in the channels 112 of the needle guide 110 are positioned at different angles (and can exit port 113 at different angles), they each can be inserted into a different location in the body without articulating, twisting, translating, or otherwise moving the assembly 100 (as illustrated in FIG. 1). Furthermore, the multiple channels 112 of the needle guide 110 (not limited to only the three shown) permit multiple biopsy needles to take samples from different locations within a body structure without additional movement of the assembly 100. This arrangement improves patient comfort during a procedure requiring the collection of biopsy samples, or the delivery of a therapy, to multiple locations within the body.

The angles of the channels in the needle guide 110 (and therefore needles 114) are determined, in part, by the locations within the body or body structure intended to be biopsied, and the depth of penetration into a body cavity by the assembly 100 that is needed to access the body structure of interest. Other factors used to determine these angles may include the ability to access a wide range of locations within the body cavity, and the need to maintain the position and/or alignment of the needles within the imaging plane of the transducer (as shown in FIG. 2). In some embodiments, the channels of the needle guide 110 and the needles 114 can also be angled to limit or prevent access to particularly delicate or sensitive body structures near the structure of interest (e.g., a nerve bundle near the sphincter during a prostate biopsy). For example, the needles can be arranged at angles from -5° (i.e., 50 below the horizontal axis), up to about 30° , although any practical angle can be used.

In one example, because the needle 114C is inserted into the channel 112 of the needle guide 110 that has a greater angle with respect to the longitudinal axis 108 than the portion of the needle guide used with needle 114A (which is substantially parallel to the longitudinal axis), the locations accessible by these two needles are different. Therefore, different regions of a body structure can be biopsied without

manipulation of the assembly **100** as a whole. In one example, an angle of a needle is selected to prevent a needle from accidental insertion into a sphincter nerve bundle proximate to the rectum and prostate. As mentioned above, regardless of the angle of the needles **114**, the needle guide **110** and the protective sheath **124** are arranged such that the needles are translated into the imaging plane of the ultrasonic transducer.

The frame **304** of the needle guide **110** is used to connect one or more of the needles **114** to the needle guide and to connect the needle guide to the cylindrical housing **104**. Additionally, the frame **304** can be used with the alignment feature **128** to position the needle guide **110** and the needles **114** with respect to the imaging plane **208**, as described above. In this example, the frame **304** is disposed within a negative alignment feature to position and align the needle **114A** with the imaging plane **208** as described above. The needle housing **308**, connected to the frame **304** and positioned within a second negative feature molded into the cylindrical housing **104** positions and aligns each of the needles **114** with the imaging plane **208** as described above.

The positioning feature **312** is connected to the frame **304** and is used to more firmly position the needle guide **110** in the alignment feature **128** by limiting movement of the frame within the alignment feature in additional directions. This reduces unintentional movement of the needle guide **110**, thereby reducing risk of misalignment between the needles **114A-C** and the imaging plane **208**. In addition to reducing this risk of unintentional movement, the positioning feature **312** can enable more precise alignment of the needles **114A-C** with the imaging plane **208**. In this example, the positioning feature **312** is approximately orthogonal to an edge of the frame **304**, thereby limiting movement of the frame in a direction parallel to the edge of the frame.

Other designs of positioning features can be used to reduce unintentional shifting of the frame **304**, and therefore the needle guide **110**, or improve alignment of the needles **114A-C** with the imaging plane **208**. In one example, the needle guide **110** is attached, fixed, or otherwise connected to the housing **308** using a clamp. In another example, the needle guide **110** is attached, fixed, or otherwise connected to the housing **308** using an elastic band that is properly positioned using a band guide groove in the needle guide and in the housing. Other types of clamps may also be used.

Also, while the needle guide **110** includes multiple channels **112** and can accommodate more than one needle **114** at a time, other examples include a single channel **112** and/or a single needle **114**.

SUMMARY

The foregoing description of the embodiments of the invention has been presented for the purpose of illustration; it is not intended to be exhaustive or to limit the invention to the precise forms disclosed. Persons skilled in the relevant art can appreciate that many modifications and variations are possible in light of the above disclosure.

Finally, the language used in the specification has been principally selected for readability and instructional purposes, and it may not have been selected to delineate or circumscribe the inventive subject matter. It is therefore intended that the scope of the invention be limited not by this detailed description, but rather by any claims that issue on an application based hereon. Accordingly, the disclosure of the embodiments of the invention is intended to be illustrative,

but not limiting, of the scope of the invention, which is set forth in the following claims.

What is claimed is:

1. An ultrasonic probe assembly comprising:

a probe housing having a proximal end and a distal end, wherein the distal end includes a face oriented at an angle with respect to a longitudinal axis extending through the proximal and distal ends;

an ultrasonic transducer array disposed on the face such that the ultrasonic transducer array is angled with respect to the longitudinal axis of the probe housing, wherein the ultrasonic transducer array is configured to operate at a center frequency of 20 MHz or greater, and further configured to produce a plurality of ultrasonic waves that form an ultrasonic imaging plane;

a needle guide having an aperture and a positioning feature, wherein the needle guide is configured to guide a needle through the aperture toward the ultrasonic imaging plane such that the needle is disposed within the ultrasonic imaging plane when the needle is extended distally through the needle guide; and

a needle guide alignment feature disposed on a surface of the probe housing and configured to maintain an alignment of the aperture of the needle guide with the ultrasonic imaging plane, wherein the needle guide alignment feature is configured to engage the positioning feature on the needle guide such that the needle guide is limited from rotating about the longitudinal axis of the probe housing.

2. The ultrasonic probe assembly of claim 1, wherein the face of the distal end of probe housing is oriented at an angle of at least 5° with respect to the longitudinal axis.

3. The ultrasonic probe assembly of claim 2, wherein the face of the distal end of the probe housing is oriented at an angle of about 13° with respect to the longitudinal axis.

4. The ultrasonic probe assembly of claim 1, wherein the needle guide comprises at least two channels configured to guide needles translated through the channels at two different angles with respect to the longitudinal axis of the probe housing.

5. The ultrasonic probe assembly of claim 1, further comprising a protective sheath configured to enclose at least the distal end of the probe housing and prevent contamination of the housing, wherein a dimensional variation of the needle guide alignment feature, a dimensional variation of the needle guide, and a dimensional variation of the protective sheath total about 250 microns.

6. The ultrasonic probe assembly of claim 1 wherein the needle guide is further configured to position a portion of the needle at a location in the ultrasonic imaging plane having a width of between about 300 and 500 microns.

7. The ultrasonic probe assembly of claim 1 wherein the ultrasonic imaging plane formed by the transducer array is generally orthogonal to the face of the housing.

8. The ultrasonic probe assembly of claim 1, wherein the ultrasound transducer array is configured as a side-fire transducer array.

9. The ultrasonic probe assembly of claim 1 wherein the ultrasonic imaging plane has a width, and wherein the needle guide is configured to receive a needle having a diameter greater than the width of the imaging plane.

10. The ultrasonic probe assembly of claim 1 wherein the needle guide is further configured to orient the needle substantially parallel to the longitudinal axis of the probe housing.

11. The ultrasonic probe assembly of claim 1 wherein the needle guide further comprises:

a needle guide housing that includes the aperture; and
a needle guide frame, wherein the positioning feature on
the needle guide is connected to the needle guide frame.

12. The ultrasonic probe assembly of claim **11** wherein the
needle guide frame includes an edge approximately orthogo- 5
nal to the positioning feature, and wherein movement of the
needle guide frame is limited to movement in a direction
parallel to the edge of the needle guide frame.

* * * * *

专利名称(译)	超声波探头和对准的导针系统		
公开(公告)号	US9655591	公开(公告)日	2017-05-23
申请号	US14/746633	申请日	2015-06-22
[标]申请(专利权)人(译)	富士胶片索诺声公司		
申请(专利权)人(译)	FUJIFILM SONOSITE , INC.		
当前申请(专利权)人(译)	FUJIFILM SONOSITE , INC.		
[标]发明人	CHAGGARES N CHRIS RIEDER ERIC MICHAEL		
发明人	CHAGGARES, N. CHRIS RIEDER, ERIC MICHAEL		
IPC分类号	A61B8/00 A61B10/02 A61B8/12 A61B8/08 A61B17/34 A61B17/00 A61B10/04		
CPC分类号	A61B8/4455 A61B8/0841 A61B8/12 A61B8/4422 A61B8/4494 A61B10/02 A61B10/0241 A61B10/0275 A61B17/3403 A61B8/445 A61B8/4444 A61B2010/045 A61B2017/00274 A61B2017/3413		
代理机构(译)	博钦律师事务所		
其他公开文献	US20160038118A1		
外部链接	Espacenet USPTO		

摘要(译)

侧射式超声波探头包括对准特征，当用于将探头与用于腔内医疗程序的针引导件连接时，该对准特征使得能够在超声换能器的成像平面中对准针。对准特征被配置成使得当保护套设置在对准特征和针引导件之间时，实现针在成像平面内的对准。该配置可以用于具有以约20MHz为中心的频率分布的高频超声阵列，以及用于医疗过程，例如活检器官或其他身体腔内结构，以及递送腔内疗法。

