



US 20090259128A1

(19) **United States**

(12) **Patent Application Publication**
Stribling

(10) **Pub. No.: US 2009/0259128 A1**

(43) **Pub. Date: Oct. 15, 2009**

(54) **MOVEABLE ULTRASOUND ELEMENTS FOR
USE IN MEDICAL DIAGNOSTIC
EQUIPMENT**

Publication Classification

(51) **Int. Cl.**
A61B 8/14 (2006.01)

(52) **U.S. Cl.** **600/459**

(57) **ABSTRACT**

(76) Inventor: **Mark L. Stribling**, Johnson City, TN (US)

Correspondence Address:

INDIANO VAUGHAN LLP
ONE N. PENNSYLVANIA STREET, SUITE 1300
INDIANAPOLIS, IN 46204 (US)

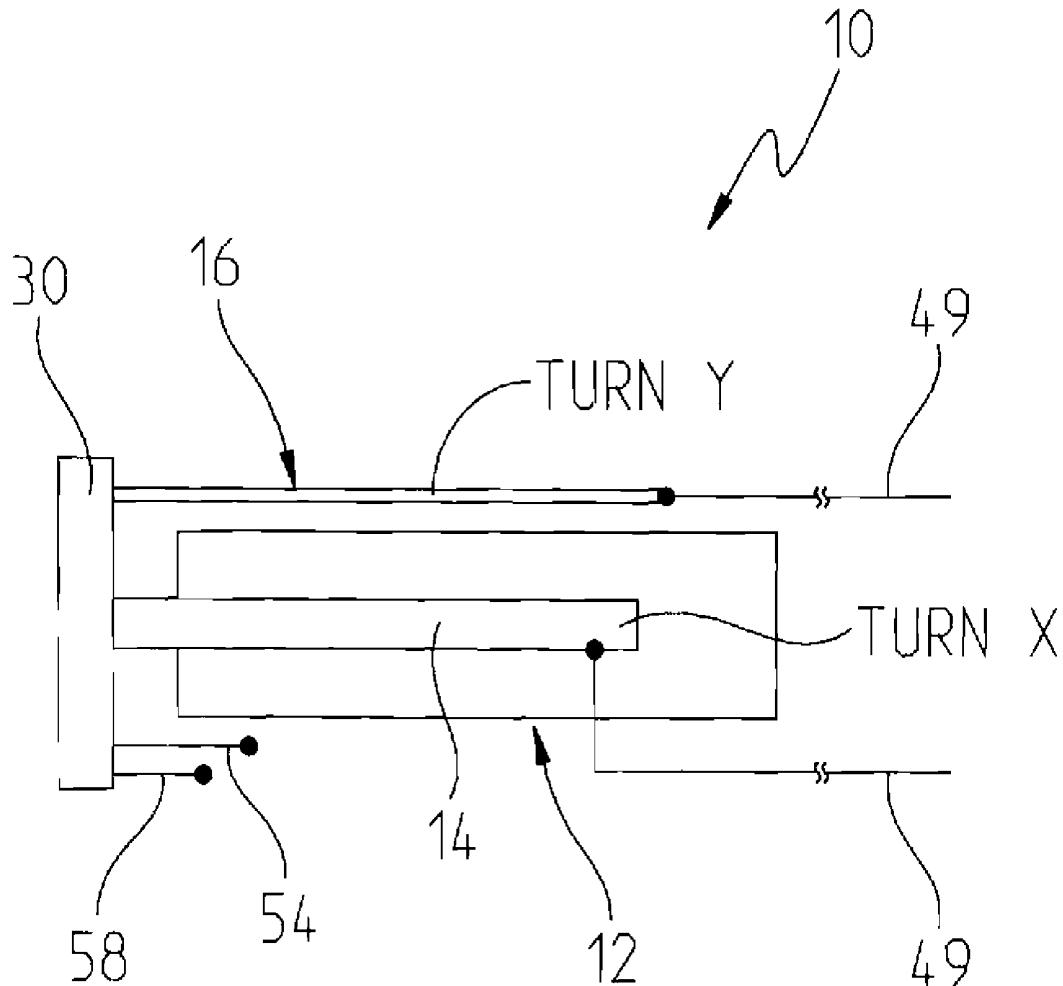
(21) Appl. No.: **12/422,766**

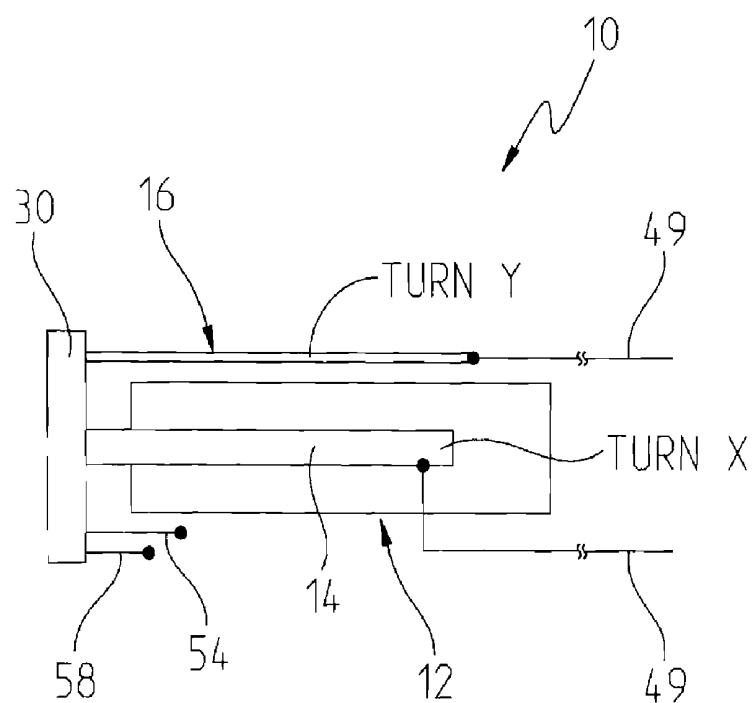
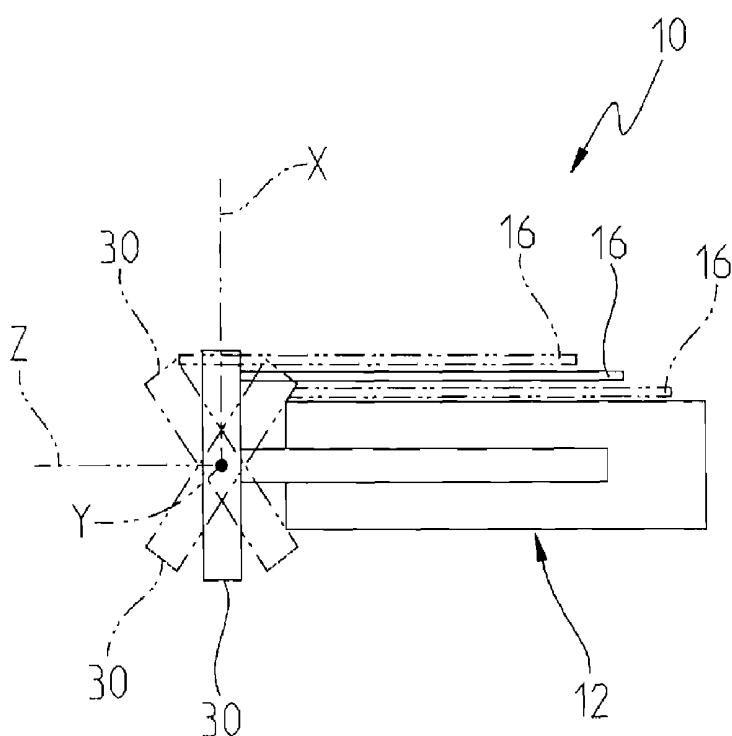
(22) Filed: **Apr. 13, 2009**

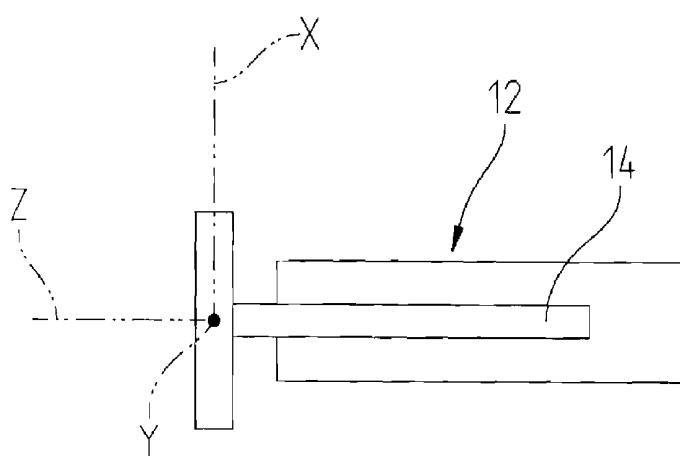
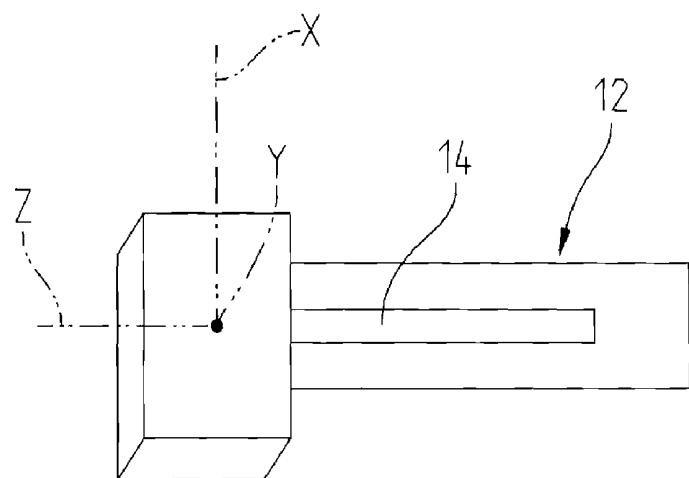
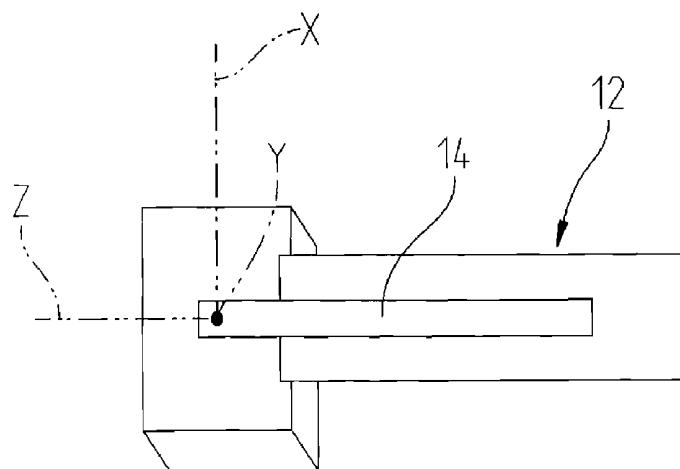
Related U.S. Application Data

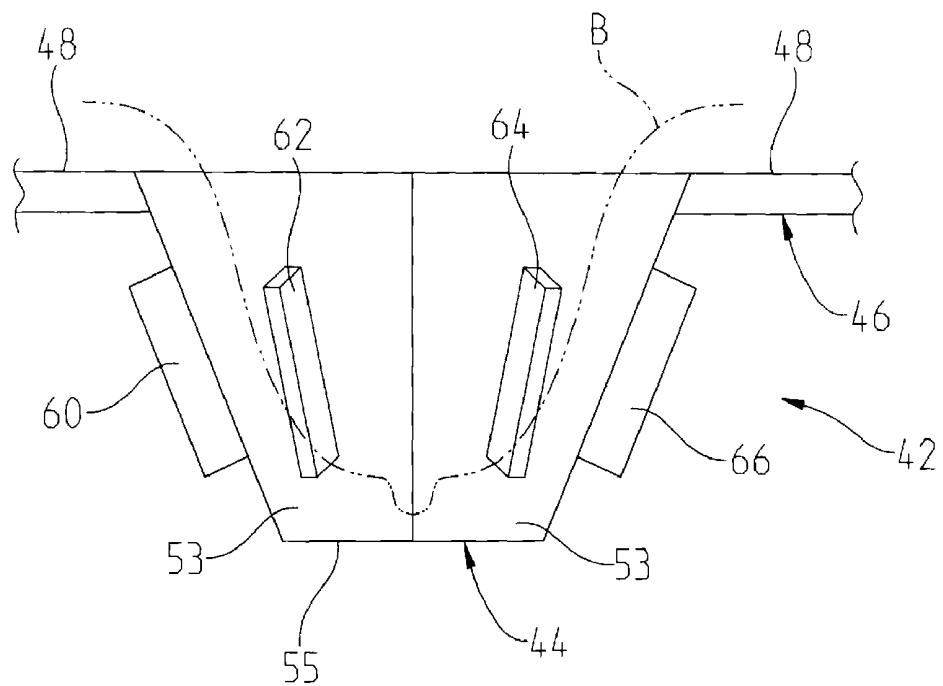
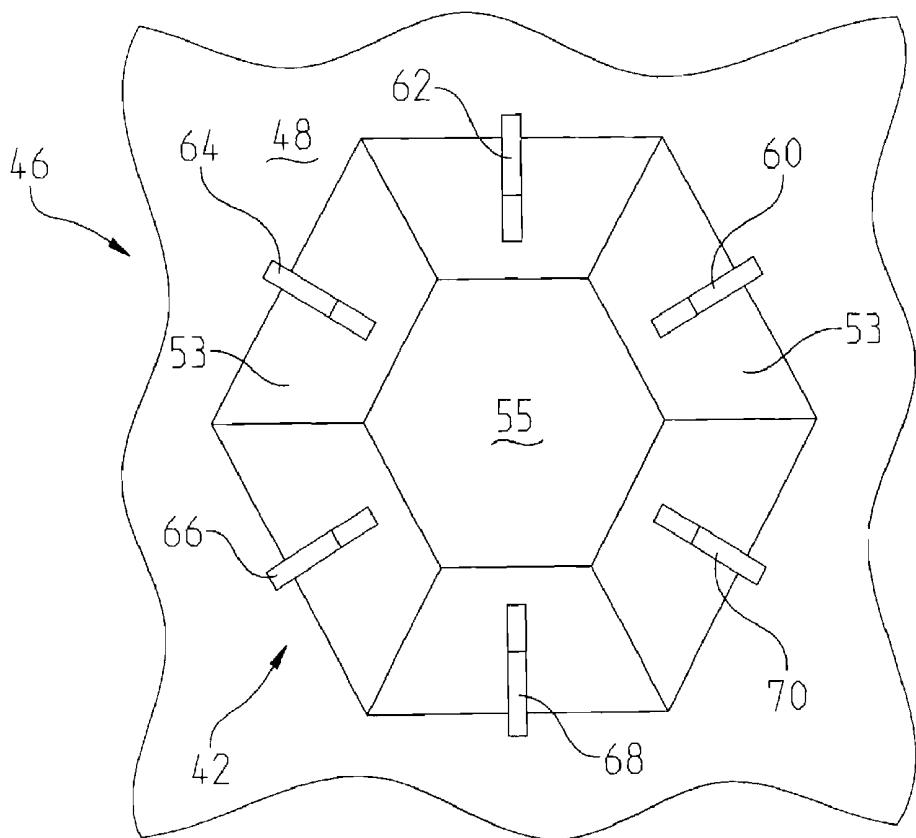
(60) Provisional application No. 61/124,064, filed on Apr. 14, 2008.

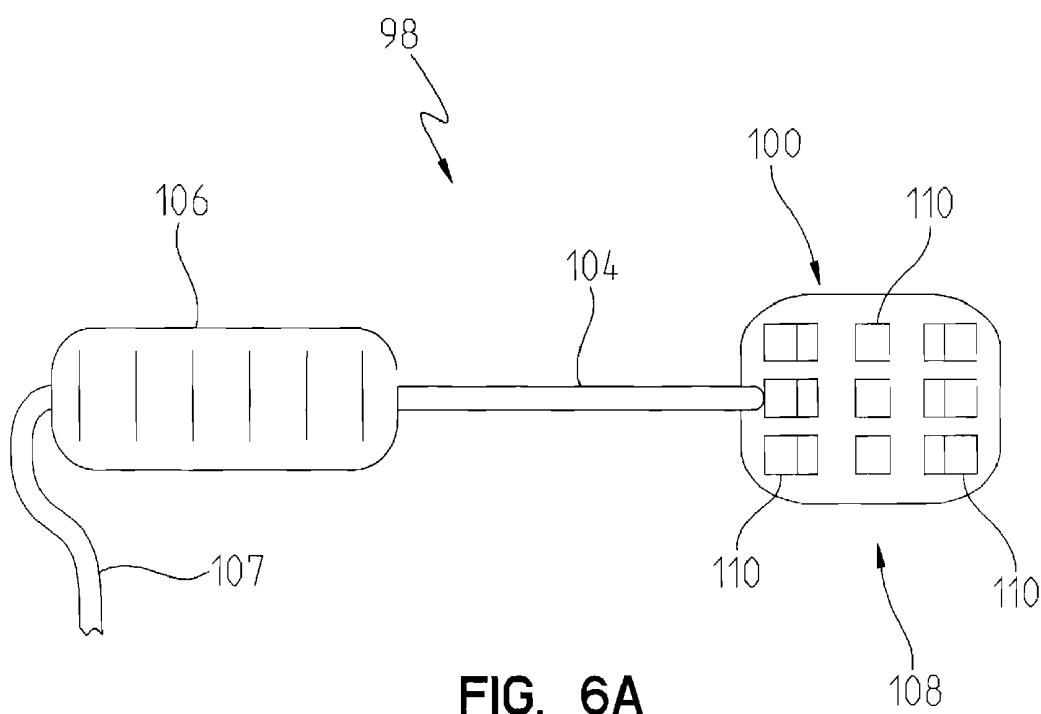
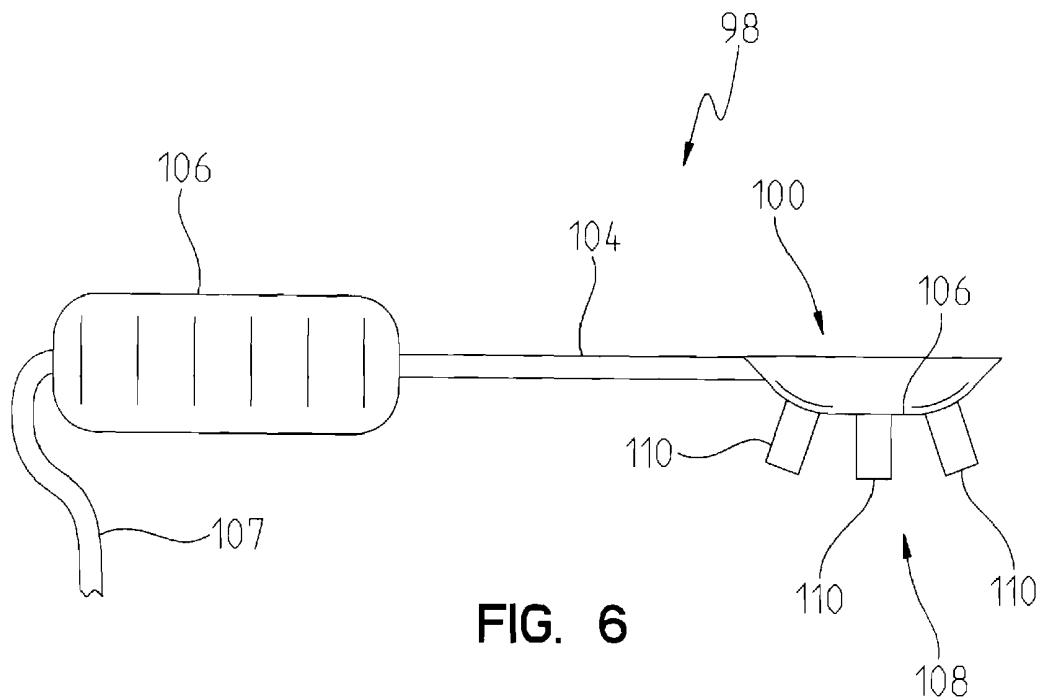
In accordance with the present invention, an ultrasound device is provided for diagnosing pathologies in a tissue of interest. The ultrasound device includes a platform member and an array of at least two ultrasonic elements coupled to the platform member. Each of the at least two elements includes a body portion and a piezoelectric crystal member. The piezoelectric crystal member has a first axis and a second axis. A first mover is provided that is capable of moving the piezoelectric crystal member about a first axis of the crystal. A second mover is provided that is capable of moving the piezoelectric crystal about a second axis of the crystal. A controller is provided for causing the first mover and second mover to move the piezoelectric crystal about the respective first and second axes for enabling the ultrasound device to capture a plurality of images at different positions of rotation about the first and second axes.



**FIG. 1****FIG. 2**

**FIG. 3A****FIG. 3B****FIG. 3C**

**FIG. 4****FIG. 5**



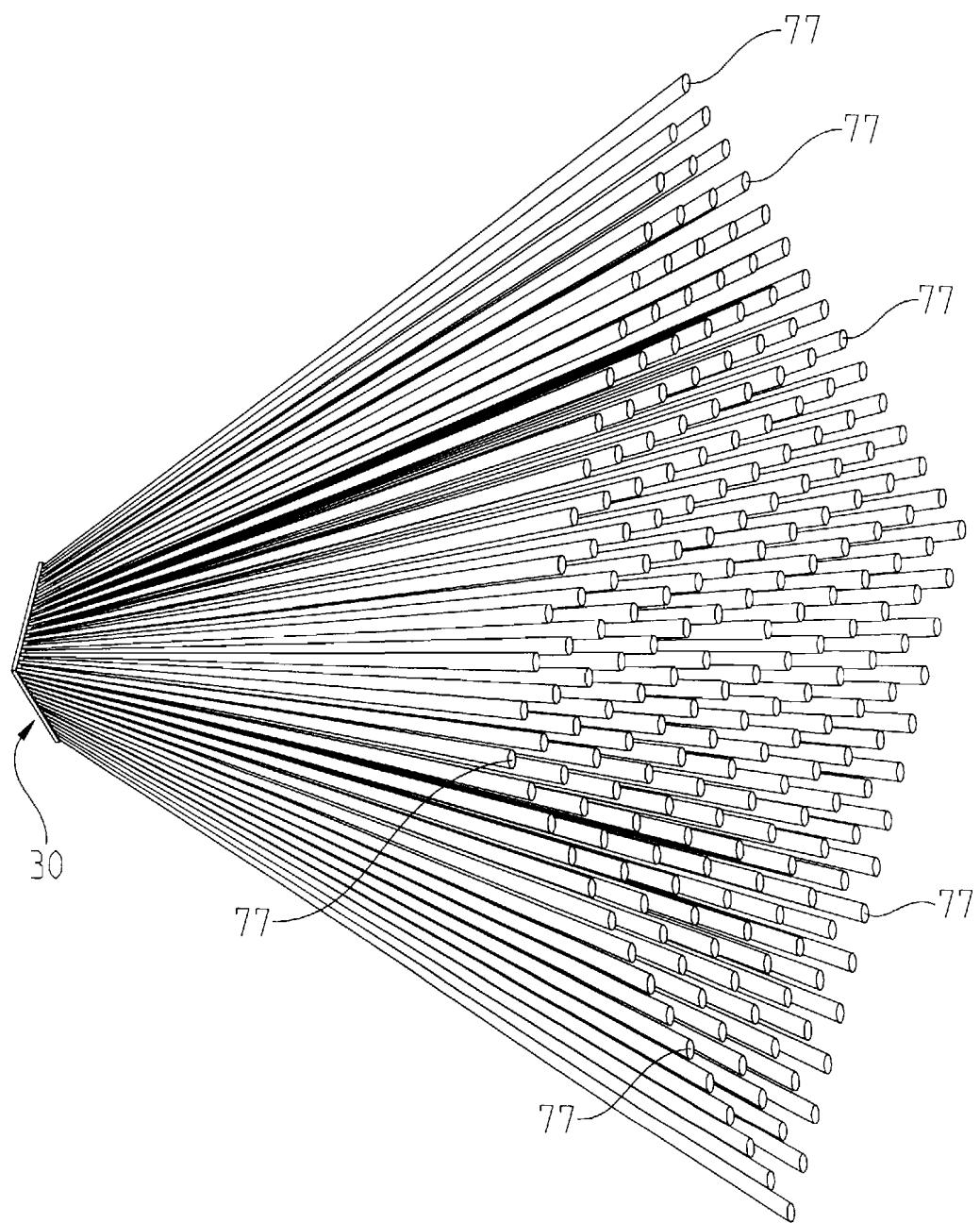


FIG. 7

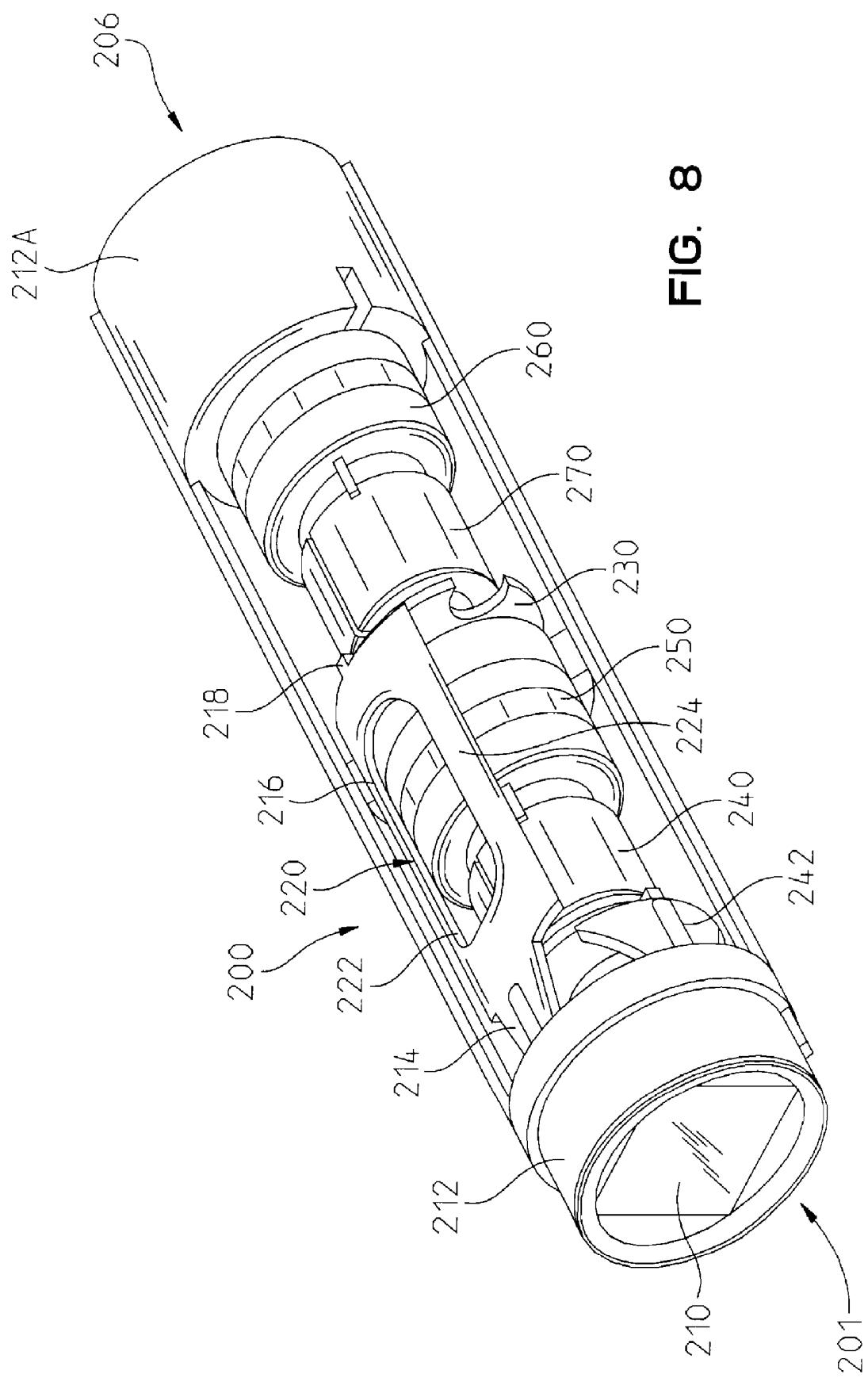
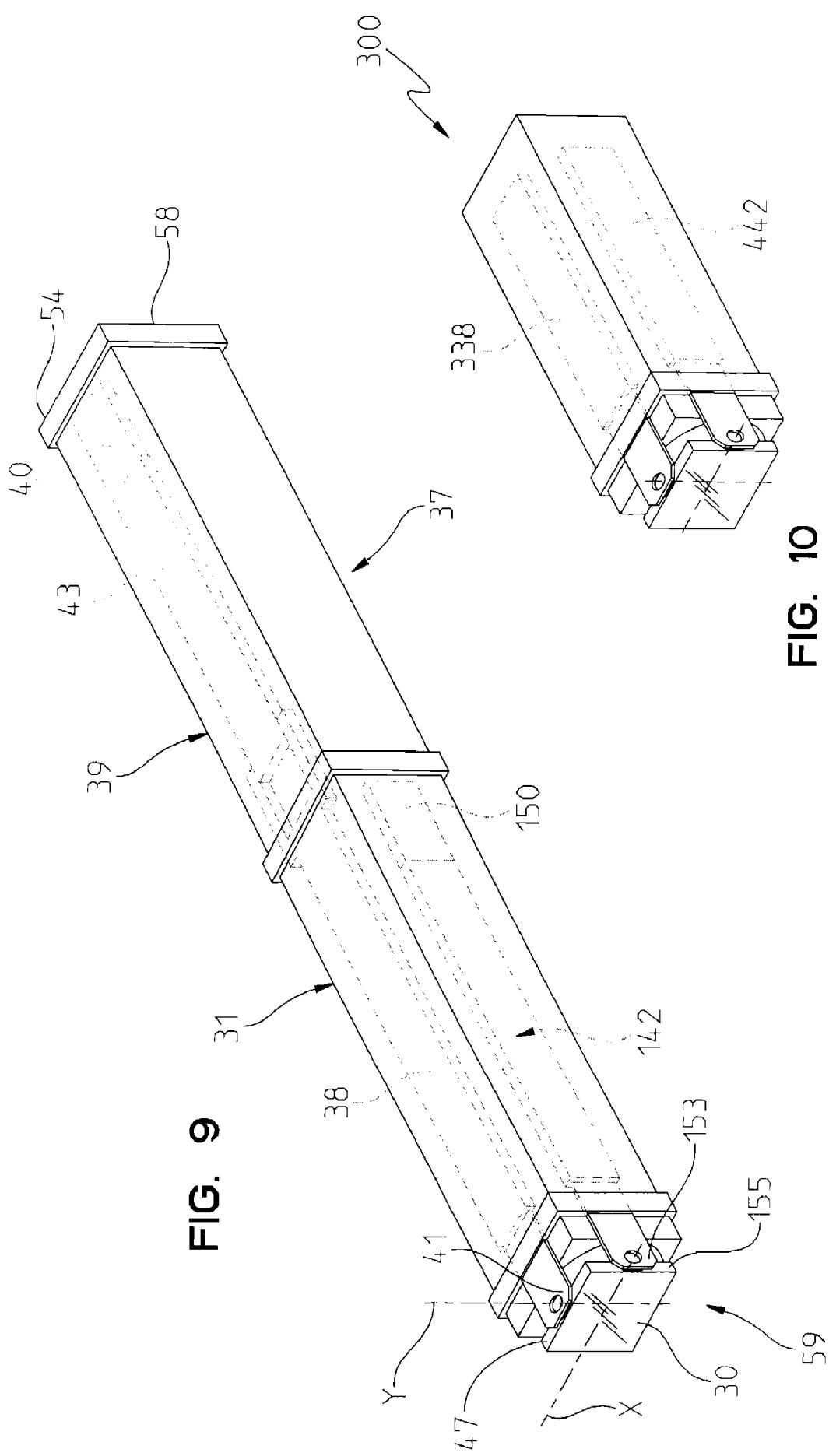
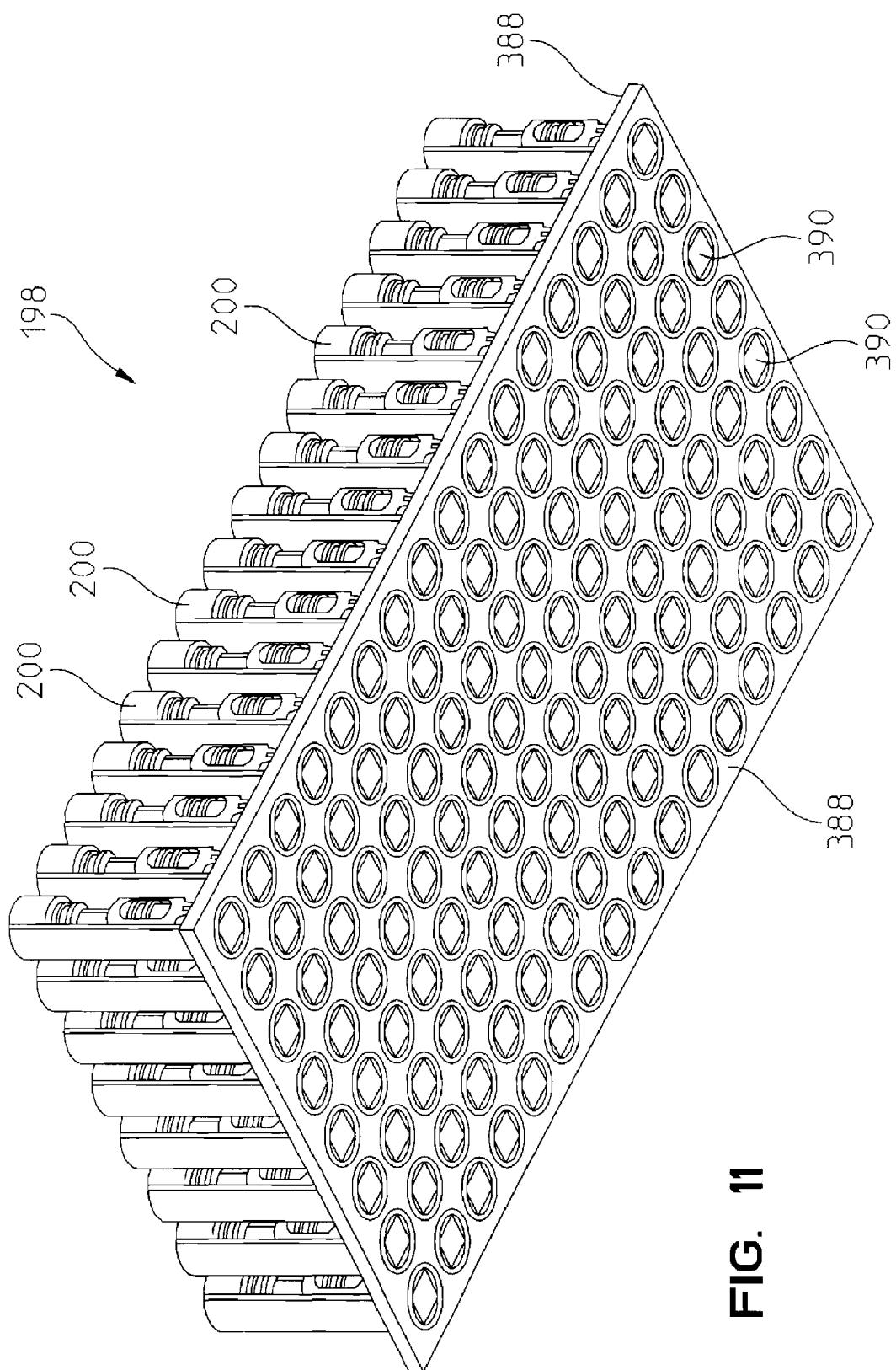
FIG. 8

FIG. 9**FIG. 10**



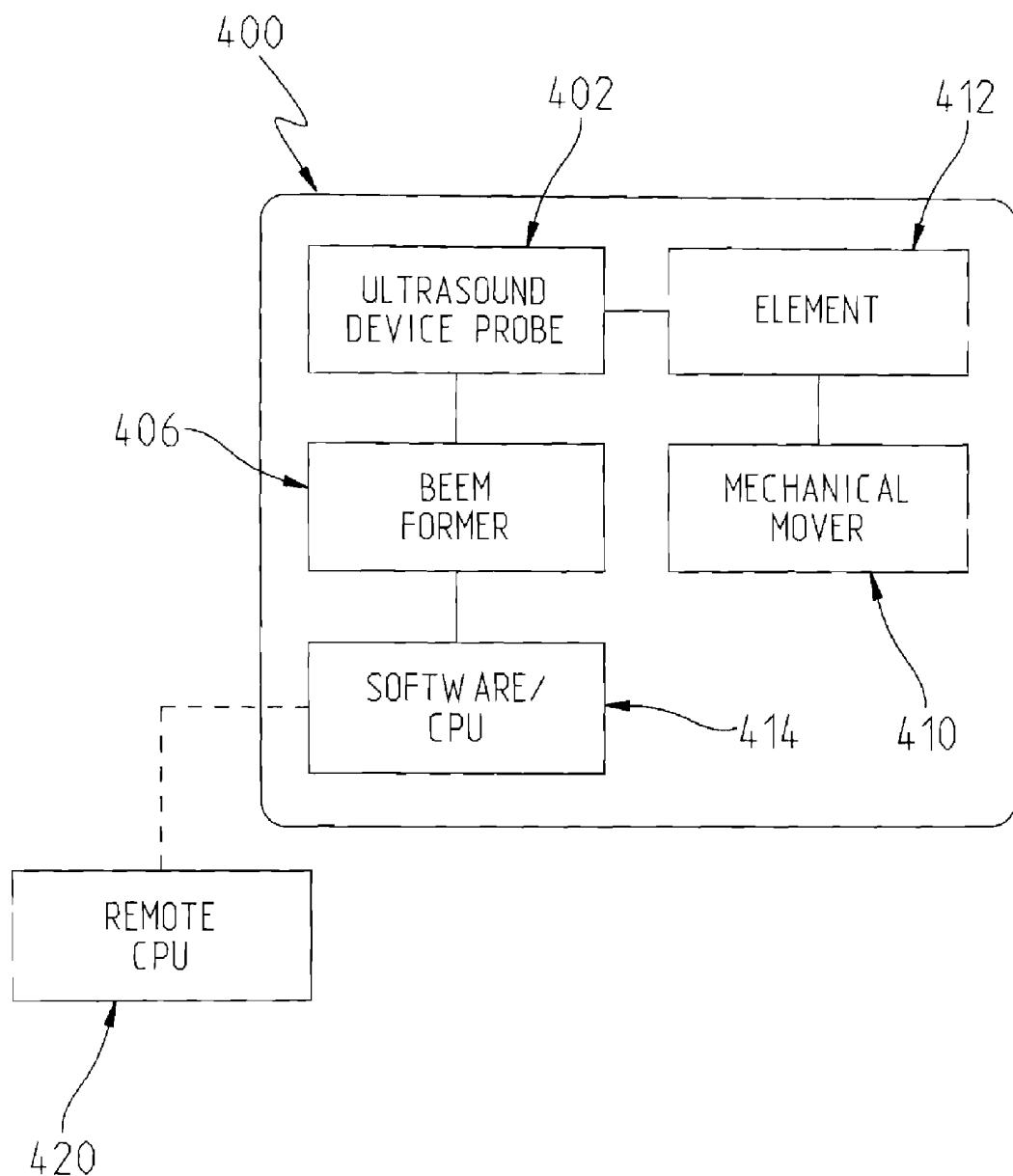
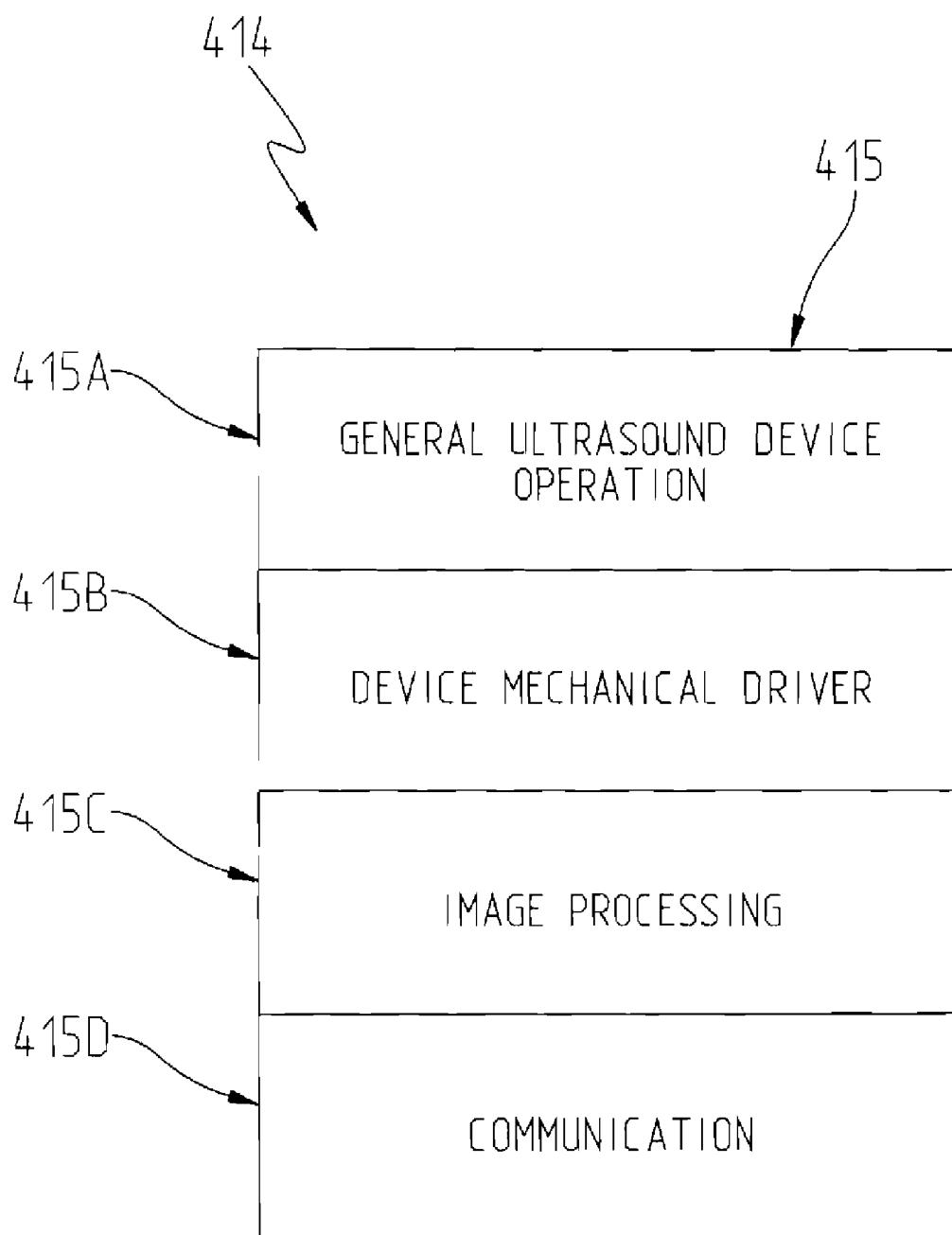


FIG. 12

**FIG. 12A**

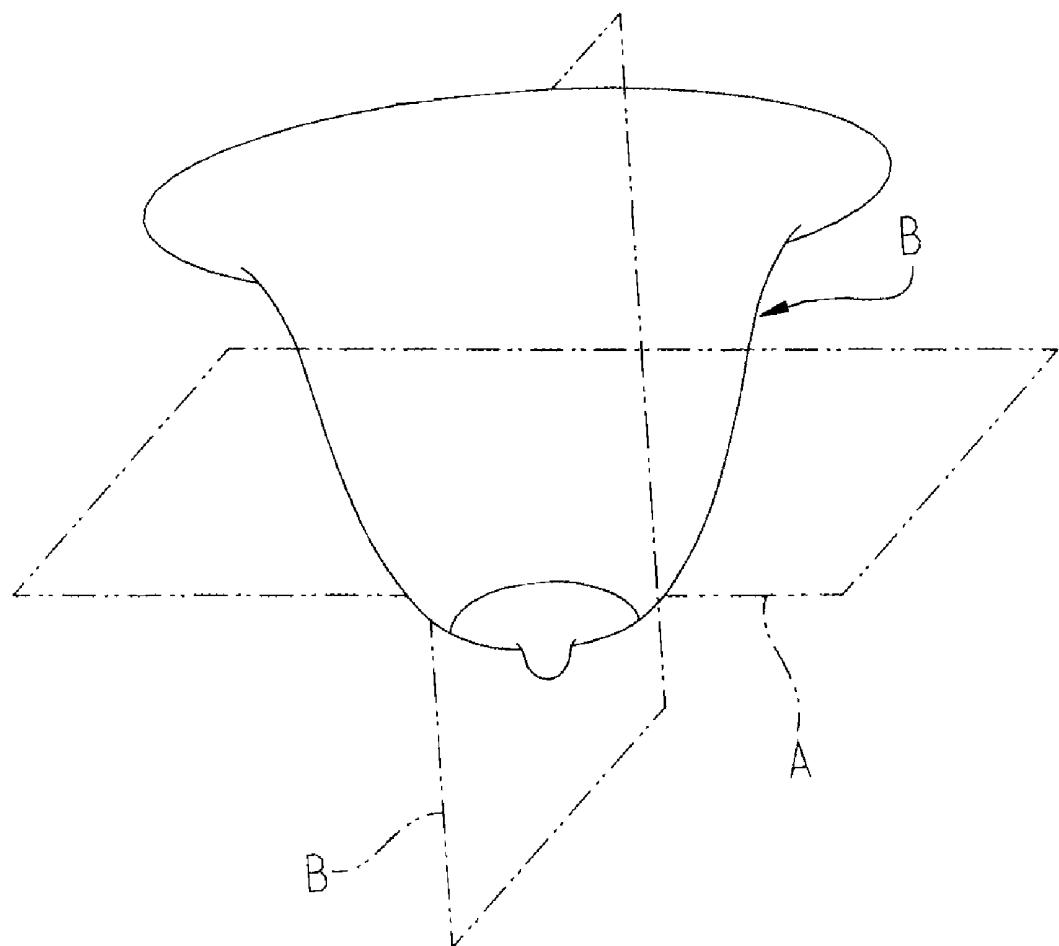


FIG. 13

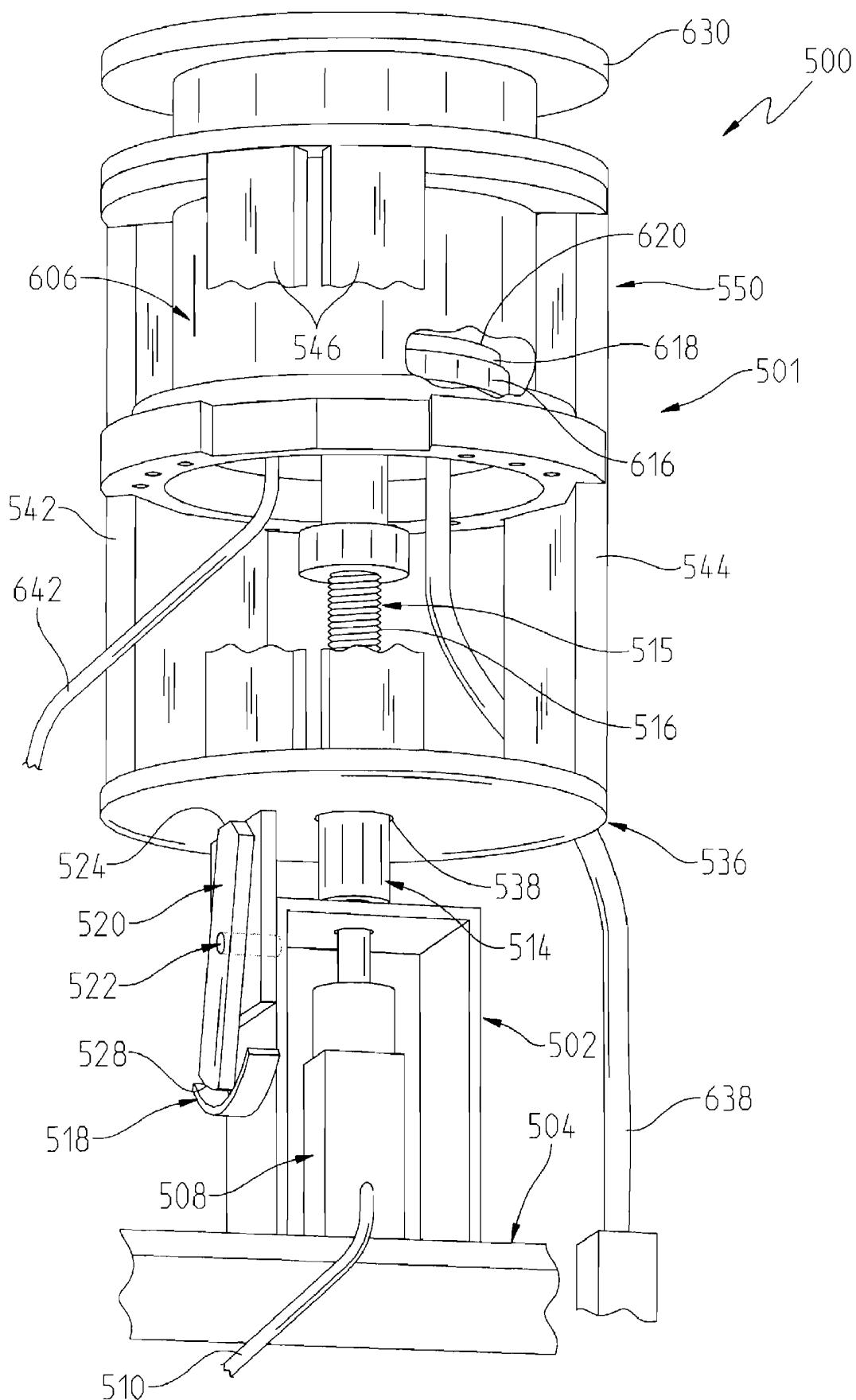


FIG. 14

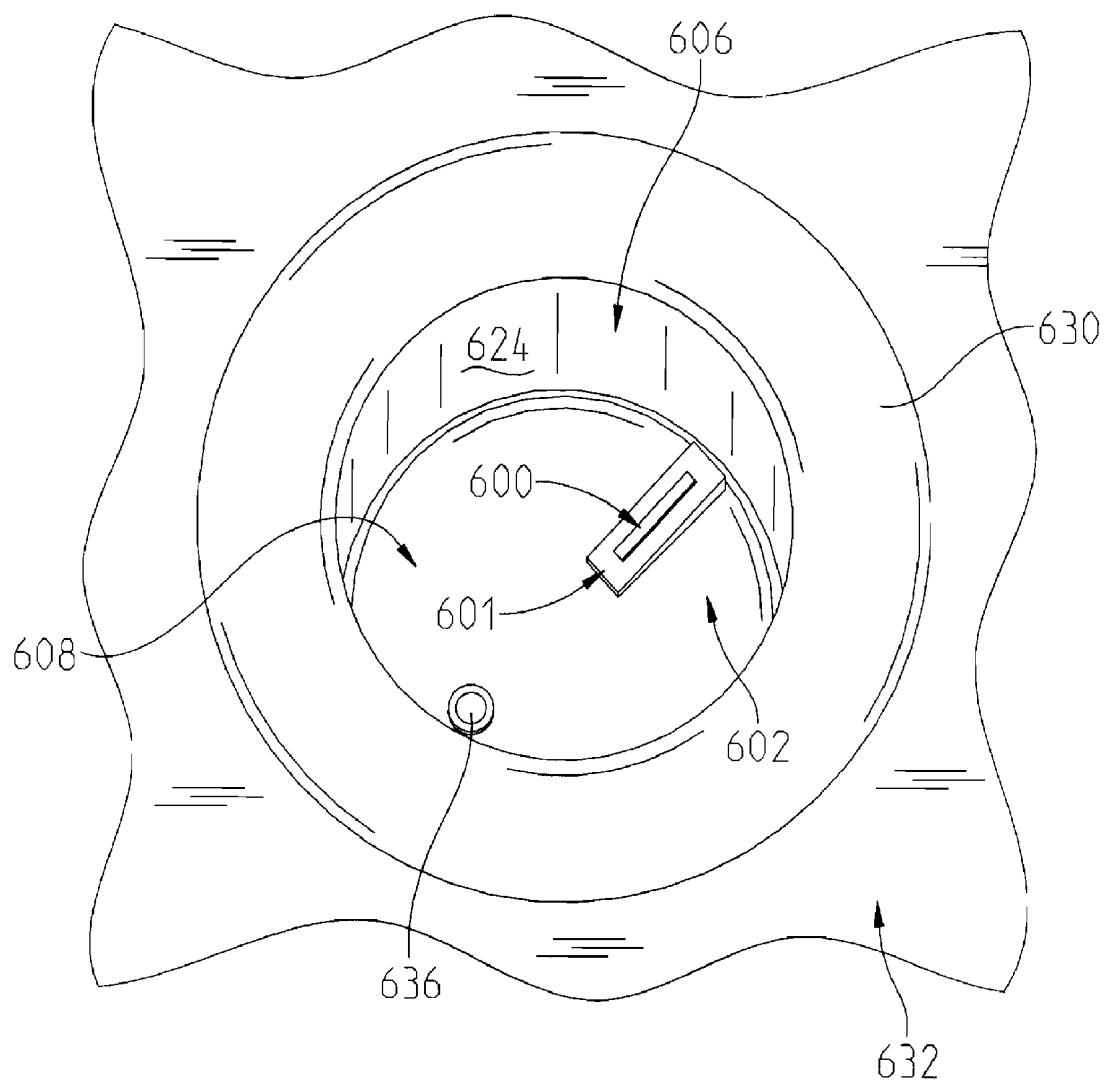


FIG. 15

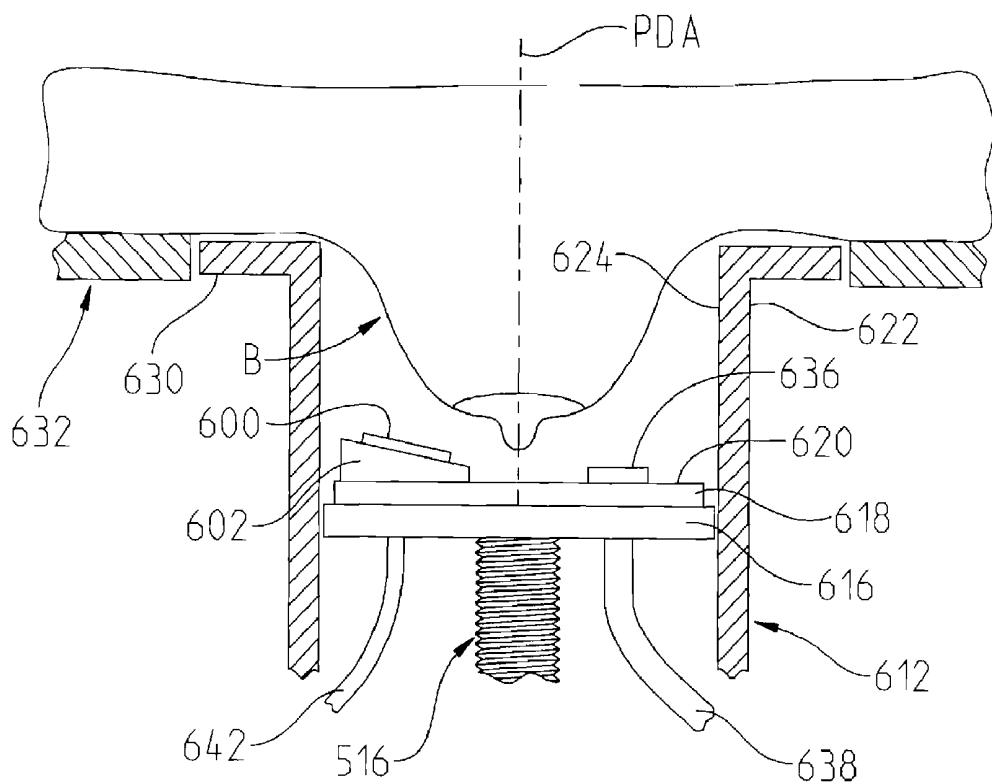


FIG. 16

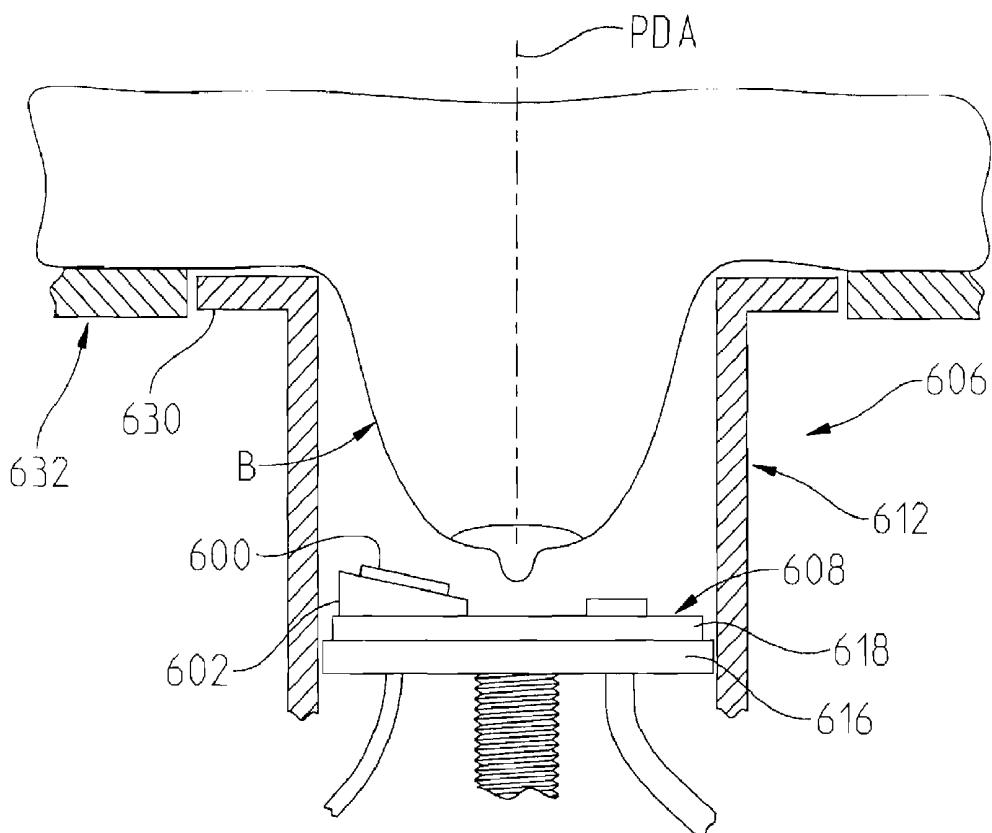


FIG. 17

MOVEABLE ULTRASOUND ELEMENTS FOR USE IN MEDICAL DIAGNOSTIC EQUIPMENT

I. PRIORITY DATA

[0001] This Application claims the benefit of U.S. Provisional Patent Application No. 61/124,064 which was filed on 14 Apr. 2008, and which is incorporated in its entirety herein by reference.

II. TECHNICAL FIELD OF THE INVENTION

[0002] The present invention relates to ultrasound equipment, and more particularly, to ultrasound equipment useable in a medical diagnostic application, such as in the examination of tissue such as breast and/or prostate tissue for determining the presence or absence of abnormal tissues, such as tumors associated with cancer.

III. BACKGROUND OF THE INVENTION

[0003] Ultrasound machines have long been used in medical diagnostic applications. For example, ultrasound machines are used to obtain real-time images of fetus in utero, and are also used to detect certain anomalies in tissues, such as the presence or absence of cancerous tissue that may exist in breasts for breast cancer detection; in prostates for prostate cancer detection and the like. Ultrasound machines are also used for detecting cancers located in the ovaries, thyroid, abdomen, liver, spleen, pancreas and kidneys.

[0004] An ultrasound machine operates through the use of sound waves that are transmitted and received in a manner similar to "radar" that can be used to create an image of a tissue of interest. The main component of an ultrasound machine is the transducer probe. The transducer probe creates and transmits the sound waves and receives the echoes by employing the piezoelectric effect. The piezoelectric effect operates through the use of one or more quartz crystals that are often referred to as piezoelectric crystals. When an electric charge is applied to these piezoelectric crystals, the crystals rapidly change shape, thereby producing sound waves that travel outwardly. When returning sound waves strike the crystals, they also change shape, and emit electric currents.

[0005] Along with the transducer probe, most ultrasound machines include a central processing unit that performs the calculations necessary to accomplish the tasks desired of the crystal. The central processing unit also contains the electrical power supplies for itself and the transducer probe, and transducer pulse controls that change the amplitude, frequency and duration of the pulse emitted from the transducer probe. An ultrasound machine may also include a display that displays the image from the ultrasound data processed by the CPU and a keyboard or pointing device (e.g. a mouse) that enables the user to input data and take measurements from the display. A data storage device, such as a hard drive, flash drive, etc., is usually also included for storing the acquired images.

[0006] Although existing ultrasound machines are highly useful diagnostic tools, room for improvement still exists to overcome certain deficiencies. Some of these deficiencies are illustrated with respect to the problems that deal with using ultrasound machines to detect abnormalities and pathologies of the breast, such as breast cancer.

[0007] The currently existing ultrasound diagnosis technology is to provide an ultrasound probe that comprises a

sensor wand or handle. Within the sensor wand or handle is contained an array of ultrasound transducers (the piezoelectric crystals). These transducers are fixedly positioned with respect to the handle. In order to capture an ultrasound image of a tissue, the ultrasound wand is moved manually by the user around the subject tissue. The wand that is typically used for detecting breast cancer comprises a 128 element linear array. In principal, this ultrasound wand operates analogously to a hand-held scanner of the type used to scan documents, as the wand comprises a sort of linear array (line) of transducers.

[0008] To perform an ultrasonic breast exam, the hand-held transducer is moved by the medical practitioner so that the linear array of transducers is moved over the breast. At the same time that the transducer-containing wand is being moved over the breast, pictures are being captured and shown on a screen (display). The technician continues to move the wand and watch the display until the technician finds something in the image that the technician believes to be an abnormal (e.g. a cancerous) tissue. In breast cancer, a cancerous tissue would tend to show up as a white calcified cell or a dark area. When the technician finds a spot or other areas of interest, the technician holds the wand stationary and captures an ultrasonic "picture" from that spot or area of interest.

[0009] After capturing an image of the area of interest, the technician may continue the examination of the remainder of the breast to determine whether any other areas of interest exist. Alternately, the technician may just try to get a few more pictures of the spot or area of interest where the technician found the cancerous tissue.

[0010] The persons who usually perform this function are sonogram ("ultrasound") technicians. Sonogram technicians are similar to x-ray technicians, as their primary job is to operate the diagnostic device to obtain those images (radiographic or sonographic) requested by the physician of the area or tissue of interest. Once the image is obtained, the image is given to an interpreting physician who then reads the pictures and makes a determination or diagnosis of whether the pictures represent the existence of a pathological condition such as cancer, a tumor or some other abnormality. In the plurality of cases, the "interpreting physician" will be a radiologist. However, physicians other than radiologists are often the interpreting physician. It should be understood that the use of the term "radiologist" in this application should not be interpreted to exclude other physicians and medical practitioners.

[0011] Currently breast cancer is usually diagnosed by employing a three-stage screening/detection process. The first stage involves a mammogram that uses x-rays for detection of pathologies. In an x-ray type mammogram, the breast is usually squeezed between a pair of plates and an x-ray is taken. The x-ray is then read by the radiologist. If the radiologist detects the presence of either a white spot or a dark area, an ultrasound is then ordered as the second stage in the screening.

[0012] Although mammograms have been used for the last thirty years as a primary screening tool to determine the existence of breast cancer, mammograms do have certain drawbacks. A first drawback to the use of mammography is that the procedure, wherein a breast is squeezed between two plates is often painful, or uncomfortable to the user. A second problem associated with mammography is that the use of mammography entails exposing the patient to radiation. Although technological improvements have reduced the

amount of radiation to which the patient is exposed, mammography still requires the use of radiation.

[0013] A more pressing problem with mammography is that its use as a diagnostic tool is rather limited, due to the limitations of the procedure. One limitation in the procedure is the mammography is only capable of providing a two-dimensional view of the breast.

[0014] Although mammography is very useful in determining whether suspicious areas exist, the presence of a suspicious area usually requires a further procedure performed by a different technique to confirm or deny the existence of cancerous tissue.

[0015] Another difficulty with mammography is that certain factors and/or conditions exist that interfere with the ability of a mammogram to provide a reliable screening because these conditions interfere with a mammogram. One example of such a condition is the presence of talcum powder, deodorants, creams or lotions that are applied under the arms or on the breasts of the patient.

[0016] Breast implants also interfere with a mammogram, as they may prevent complete visualization of the breast. Further, previous breast surgery can also interfere with an interpretation of a mammogram. Additionally, breast changes that may occur during menstruation interfere with a mammogram. Another condition that interferes with mammograms involve the existence of dense breast tissue, that often is characteristic of young women, and especially women under 30.

[0017] In addition to screening mammograms, diagnostic mammograms also exist. A diagnostic mammogram is an x-ray exam of the breast in a woman who either has a breast problem, such as a lump, nipple discharge, or has something abnormal found during a screening mammogram.

[0018] A diagnostic mammogram differs from a screening mammogram, as more pictures are taken to better and more carefully study the area of concern. Often, special pictures are enlarged to make small areas of suspicious breast tissue larger and easier to evaluate. Additionally, other types of x-ray pictures can be taken, the nature of which depends upon the type of problem and the location of the problem in the breast.

[0019] For a good discussion of other breast cancer detection techniques, including the use of mammograms, ultrasounds, MRIs and other techniques for imaging the breast, see, American Cancer Society "Mammograms and Other Breast Imaging Procedures", www.cancer.org, 2005, the text of which is incorporated herein by reference in its entirety.

[0020] After a mammogram has been performed, an ultrasound is often used as the second stage of the screening. If the ultrasound comes back positive, the third step in the process is to perform a tissue biopsy. Although this method is the current state-of-the-art, there are several deficiencies with it.

[0021] Another example of detection through ultrasound relates to the manner in which prostate cancer is detected. In a prostate cancer ultrasound procedure, a probe is inserted rectally. The probe generally comprises a cigar tube-shaped having a rounded distal end for facilitating insertion. Along the outer surface of the "tube" is a linear array of ultrasound transducers. The cigar-shaped wand is inserted rectally until it is positioned adjacent to the prostate. When placed in this position, the ultrasound array is preferably positioned so that it is facing the wall of the large intestines that is next to the prostate. The linear ultrasound array is then employed to take a linear array of ultrasound pictures while the doctor or sonogram technician manipulates the wand in order to look at

various parts of the prostate. This manipulation occurs by rotating the cigar tube about its axis so that the technician can capture pictures of various parts of the prostate.

[0022] From this point on, the procedure is similar to a breast exam procedure as the technician rotates the wand to capture views of the entire prostate until the technician has either viewed the entire prostate (and found nothing abnormal) or else the technician has located an area of tissue having a cancerous appearance or that is otherwise the subject of interest, be it a cyst, cancer cells, etc. The technician then captures pictures of the subject of interest. The captured pictures are then given to an interpreting physician who "reads" the ultrasonic picture to make a diagnosis from the picture.

[0023] Several problems exist with this method of performing an ultrasound procedure. Many of these problems spring from the fact that the pictures or images captured by the ultrasound are difficult to interpret and do not often present a very good picture of what is going on in the tissue or organ of interest.

[0024] In traditional ultrasound, the images that are acquired from the linear transducers are two dimensional images that take a picture of a paper thin "section". The problem with such an image is that it does not place the image in context with what the ultrasound is actually "looking at" vis-a-vis the tissue that is next to it. This two dimensional, thin section technique may lead the technician or radiologist to miss abnormal anatomical features completely if the ultrasound "picture" is taken so that it is looking at the right area and at the right angle. When something abnormal is found, the abnormal tissue may be shown in the picture at an angle that presents a view that does not portray the abnormality well.

[0025] One way to understand how mis-characterizations exist is to imagine that you are using such a linear array of transducers to look at a soccer ball. Because of the nature of the linear array, you are only permitted, at any one time, to look at a thin slice of the soccer ball. Hence, if you are looking at a thin slice on the left side of the soccer ball, you may miss an abnormality on the right side of the soccer ball. This inability of current ultrasounds to obtain an integrated picture of the entire organ of interest is one of the major deficiencies of current ultrasound devices.

[0026] One of the problems with known current ultrasound systems is that it is very difficult, if not impossible, to obtain a three-dimensional image. Even though a three-dimensional image could be obtained in theory by using a moving probe, the movement of the probe manually (which is currently being done) does not provide precise enough movements to enable even a sophisticated software package to reliably stitch together the photographs into a three-dimensional image.

IV. SUMMARY OF THE INVENTION

[0027] In accordance with the present invention, an ultrasound device is provided for diagnosing pathologies in a tissue of interest. The ultrasound device comprises a platform member and an array of at least two ultrasonic elements coupled to the platform member. Each of the at least two elements includes a body portion and a piezoelectric crystal member. The piezoelectric crystal member has a first axis and a second axis. A first mover is provided that is capable of moving the piezoelectric crystal member about a first axis of the crystal. A second mover is provided that is capable of moving the piezoelectric crystal about a second axis of the crystal. A controller is provided for causing the first mover

and second mover to move the piezoelectric crystal about the respective first and second axes for enabling the ultrasound device to capture a plurality of images at different positions of rotation about the first and second axes.

[0028] Preferably, the first and second axes of the piezoelectric crystal comprise respectively an x-axis and a y-axis, wherein the mover is capable of moving the piezoelectric crystal about the x-axis, and a second mover is capable of moving the piezoelectric crystal about the y-axis.

[0029] Imaging software is preferably provided for correlating the plurality of images to produce at least one of a thin section image and a three-dimensional image. The imaging software should be capable of producing a plurality of thin section images that show parallel planes of the tissue of interest, and/or show views of a particular tissue of interest from different aspects and angles.

[0030] The first mover preferably comprises a band that is comprised of a material capable of expanding and contracting under the influence of energy applied to the band, wherein the expansion and contraction of the material of the band moves the piezoelectric crystal about the first axis. Most preferably, the band is comprised of a metal material, and includes a first end coupled to the body portion of the ultrasonic element, and a second end coupled to a first edge portion of the piezoelectric crystal. The second mover can be constructed similarly to the first mover.

[0031] The device also should include a tissue receiving member for receiving a tissue member, so that images can be taken of the tissue of interest. The platform is fixedly coupled to the tissue receiving member, and the body portions of at least two elements are fixedly coupled to the platform member. The piezoelectric crystal members are movable relative to the platform in the body portion.

[0032] In one embodiment, the tissue receiving member comprises a cup that itself comprises the platform to which the array of at least two ultrasonic elements are coupled. The array of at least two ultrasonic elements preferably comprises at least four arrays of at least two ultrasonic elements that are circumferentially arrayed around the cup to enable the ultrasonic elements to capture images fully around an axis of the tissue of interest.

V. BRIEF DESCRIPTION OF DRAWINGS

[0033] FIG. 1 is a schematic view of an individual motorized ultrasound element;

[0034] FIG. 2 is a schematic representation of the movement of the ultrasound by the motor in two of the degrees of freedom, each way about the Y axis;

[0035] FIGS. 3A, 3B and 3C are schematic representations of movement of the piezoelectric crystal by the motor showing movement around the X axis;

[0036] FIG. 4 is a schematic side view of an ultrasound array that is used with a breast specific apparatus for performing ultrasound on a breast;

[0037] FIG. 5 is a bottom view of the ultrasound probe apparatus useable in examining a breast;

[0038] FIG. 6 is a schematic top view of a probe useable for an internal body part, such as a prostate;

[0039] FIG. 6A is a schematic side view of the probe of FIG. 6;

[0040] FIG. 7 is a schematic representation to illustrate the data points taken by the moveable ultrasound probe of the present invention;

[0041] FIG. 8 is a first embodiment cylindrically shaped ultrasound probe element of the present invention;

[0042] FIG. 9 is a second embodiment, relatively longer, rectangularly cuboid ultrasound probe element; and

[0043] FIG. 10 is a third embodiment that comprises a relatively shortened rectangular cuboid probe element;

[0044] FIG. 11 shows a multi-element array of cylindrical elements that are all disposed on a common platform, but each of which is individually moveable with respect to the remainder of the elements;

[0045] FIG. 12 is a diagrammatic view of the primary components of the ultrasound device of the present invention;

[0046] FIG. 12A is a schematic representation of the software functionalities used in connection with the present invention;

[0047] FIG. 13 is a schematic view of a body part illustrating exemplary planes through which an ultrasound picture can be taken;

[0048] FIG. 14 is a side view of an alternate “movable platform” embodiment of the present invention;

[0049] FIG. 15 is a top perspective view of an organ receiving cup of the movable platform embodiment of the present invention;

[0050] FIG. 16 is a side, schematic view of the organ receiving cup of the platform embodiment showing the cup base in a relatively raised position to reduce the relative volume of the interior of the organ receiving cup; and

[0051] FIG. 17 is a side schematic view of the organ receiving cup, similar to FIG. 16, except wherein the cup base is shown in a relatively lowered position to increase the relative volume of the interior of the organ receiving cup.

V. DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENT

[0052] The present invention comprises an ultrasound device and in particular an ultrasound device particularly well suited for use in medical diagnostic applications. The ultrasound device 198 is comprised of a plurality of individual ultrasound elements 200 (FIG. 11). The ultrasound elements 200 are placed in a fixture 388, and include crystals 390 that are individually moveable with respect to the fixture 388.

[0053] One advantage of the present invention is that each of the individual elements 200 are individually moveable on an individual basis.

[0054] In FIG. 12, ultrasound device system 400 is shown schematically. The ultrasound device 400 includes an ultrasound probe 402 that is designed to employ ultrasonic waves to enable a user to perform medical diagnoses. The ultrasound device 400 includes a digital beam former 406 that controls the beam produced by the ultrasound device 400. A mechanical driver 410 is provided for each of the individual ultrasound elements 412 that contain a piezoelectric crystal for generating and receiving ultrasound sound waves. Software for controlling the operation of the device 400, along with a CPU 414 is also provided. Among the elements or modules of the software is a mechanical driver module (or a mechanical module functionality routine within the software).

[0055] The mechanical driver module of the software communicates with the ultrasound device 400 for determining the movement of, and directing the movement of the device 400 as it moves the elements 412 in their four degrees of freedom (See FIG. 1-3C). The software containing central processing unit 414 is provided for processing the images captured by the device. The CPU 414 that captures the information received

by the elements also has the capability of transmitting the information to a remote CPU 420 through traditional means such as the Internet, direct link connection, Network connection, wireless connection and the like.

[0056] Turning now to FIG. 12A, the various software modules 415 that are contained within the CPU 414 are shown in a highly schematic manner. The various software modules (or functionalities) are shown in FIG. 12A as comprising four primary functionalities. Depending upon the software architecture used, the various functionalities can be part of a single program, or alternately, can be four separate programs, or some combination thereof.

[0057] The functionalities include a general ultrasound device operating functionality 415A. This functionality would be designed primarily to control the operation of the device 400 itself. In addition to this, a device mechanical driver 415B is provided to control the mechanical movement, and mechanically moving and mover components of the device 400. Imagine processing software 415C is provided for enabling the images taken by the ultrasound device to be processed into an image useable by the user. Additionally, the image processing software 415C should include some means for permitting the user to manipulate the image to better view those items within the image that the user believes to be important.

[0058] Further, the image processing software 415C can include a functionality, similar to one that one might find in a program such as Adobe® PhotoShop®. For example, the image processing software 415C, may enable the user to convert the image from black and white to color, change the size of the image, cut and/or crop the image, increase the brightness or the contrast in the image, sharpen the image, or perform one of several other functions to the image to enhance the ability of the image to highlight the pathologies contained within the tissue being shown, or otherwise make the image more useable or more aesthetically pleasing to the user.

[0059] A fourth functionality that should be included within the CPU 414's software package is a communications functionality 415D. This communications functionality 415D is provided to permit the CPU 414 to communicate with the remote PC 520, or other devices that are either within the CPU's 400 network, or are external to the network.

[0060] One functionality that the communication software should be able to perform is to enable the CPU 414 and hence the device 400 to transmit information to remote CPU 420.

[0061] The heart of the ultrasound device 400 resides in the individual ultrasound elements 10 that are shown in FIGS. 1-3C. Turning now to FIGS. 1-3c, an individual ultrasound element 10 includes a body portion 12 to which a piezoelectric crystal 30 is coupled. The piezoelectric crystal 30 is the component that actually emits the sound of a certain frequency or wave length used with the ultrasound. A pair of motors, including a "Turn X" motor 14 and a "Turn Y" motor 16 are provided for moving the crystal 30. Collectively, motors 14, 16 comprise a piezo motor that cause the crystal 30 to move in four degrees of freedom. The motors 14, 16 comprise a pair of wire-like straps 14 and 16. Piezo strap motor 14 is coupled on one side of the generally square crystal 30 and piezo electric strap motor 16 is coupled to another of the side edges of the crystal 30. Through contraction and expansion of the strap 14, the Piezo crystal 30 can be moved in a direction so that it rotates essentially around axis X, as shown in FIGS. 3A-3C. Through the contraction and expansion of strap 16,

the piezo crystal 30 can be rotated about an axis Y, shown in FIG. 2. Although the rotation of the crystal is described as being around the X axis and the Y axis, it will be appreciated that the rotation could also be about the Z axis, if that were deemed desirable by the user or manufacturer.

[0062] A first wire 49 (FIG. 1) is coupled to the Turn X piezoelectric motor strap 14 mechanical driver that sends a signal to the piezoelectric motor strap 14 to expand or contract, and thereby move to change the orientation of the crystal 30 about the X axis. A second wire 50 is coupled to the second piezoelectric motor strap 16, to cause second strap 16 to move, to cause the crystal 30 to rotate its orientation about axis Y as shown in FIG. 2.

[0063] A send wire 54 and a receiver wire 58 are also coupled to the piezoelectric crystal 30. The send wire 54 is used to send information to the piezoelectric crystal 30. The information sent is usually a signal to tell the piezoelectric crystal 30 to send out an acoustical sound signal into the tissue of interest. The receive wire 58 is provided for receiving signals that bounce back to piezoelectric crystal 30 and transmitting these signals ultimately to the CPU 400.

[0064] Ultrasound works somewhat similarly to a sound-based radar system where a signal is sent out and is received by the piezoelectric crystal. Through processing performed by appropriate software, by sending and receiving signals and comparing the times, frequencies and types of signals sent and received, one can detect the presence or absence of various tissue types that the signal encounters in its path away from and back to the ultrasound piezoelectric crystal 30. From these signals, and their processing, an image can be constructed from and by the imagine processing software 415D.

[0065] In operation, during the acquisition of data information, the ultrasound element 30 is constantly sending out signals and receiving signals in order to provide the underlying data from which the image is built. In certain living tissues and moving organisms, this image can change which reflects movement of the tissue, such as the movement incident to the beating of a heart. While this is occurring, the piezoelectric crystal 30 is moved so that it rotates about the X axis and rotates the Y axis. Preferably, it is capable of 20 different positions of rotation along the X axis and 20 different positions of rotation along the Y axis. Turning now to FIG. 7, when the crystal has gone through its entire sequence of rotation around the X axis and then through the entire sequence of rotation around the Y axis, image information is retrieved from an array of data points that are represented by the array of end points 77 shown in FIG. 7.

[0066] Because the ultrasound element 30 is capable of movement, the ultrasound element 30 sends information back to the software 415 converts the information it receives from the array of ultrasound elements into a three-dimensional picture of the tissue sample of interest. As such, in order to make this reconstruction, software is needed that is capable of assembling a large number of images together into a coherent three-dimensional image. In order to assemble this data into a three-dimensional image, the computer or image processing software 415C needs: (1) information relating to the image itself; and (2) information that relates to the position of the sensor, so that the position at which the image was "taken" is known by the software 415C. From this information, the software 415C can determine that a particular feature on an image represents a certain point in three-dimensional space in the tissue sample.

[0067] One way to understand this is to look at the breast probe ultrasound device that is shown in FIGS. 4 and 5. In FIG. 4, the breast prototype ultrasound device 42 is shown as comprising a generally a six-sided tapered cup 44 that is shown in the top view of FIG. 5. The cup 44 is imbedded in an examination table 46, so that the cup 44 extends below the surface 48 of the table 46. The cup 44 is sized and positioned so that the patient can lay face down, with his/her front side (chest) on the surface 48 of the table 46, with his/her breast B extending into the interior of the cup 44. The cup 44 is preferably water-tight since the interior 50 of the cup is preferably filled with a media as a medium for the ultrasonic waves to travel in during use. Preferably the medium comprises a liquid medium such as water, but can also comprise another type of medium suitable for use with ultrasound, such as a jelly-like medium. Preferably, the water (or other media) is heated up to close to body temperature to improve the comfort level of the test subject.

[0068] The cup can be frusto-pyramidal and include six side panels 53 and a hexagonal base panel 55.

[0069] Along each of the six side panels 53 of the six-sided cup is disposed a plurality of moveable ultrasound element arrays 60, 62, 64, 66, 68, 70. Each of these arrays 60-70 of moveable ultrasound elements comprises an array of two elements across by 100 elements down (200 total elements). The elements 200 (See FIG. 11) will preferably extend along a significant length of each panel 53, so that the arrays 60-70 can capture images of the entire length of the breast B. This 100×2 array may appear similar to the array 198 of elements 200 shown in FIG. 11, but of course, much narrower and much longer than the array 198 of elements 200 shown in FIG. 11. As such, six of these arrays 60, 62, 64, 66, 68 and 70 are contained on the ultrasound device 42.

[0070] During the time the ultrasound is being taken, each of the elements 200 on each of these arrays 60-70 is capable of being moved individually and often are moved individually. However, the elements 200 on any particular array, such as the elements on array 66, while being moved individually are preferably all moved synchronously. Turning to FIG. 7, each of the 100×2 (200 elements) capable of sending and receiving signals that can be used to capture a plurality of images at a plurality of points so that each element captions a multi-point image similar to the image representation shown in FIG. 7 that results from the elements being moved along the X axis and about the Y axis.

[0071] At the same time this is occurring, the same arrays (e.g. 64 and 62) are taking their pictures of the tissue sample of the breast. As can be appreciated, the images taken from the different arrays 60-70 will all be different, because the arrays 60-70 are all "shooting" their images from a different position and at a different angle relative to the tissue of interest. However, since the arrays 60-70 are all shooting the same tissue sample, the images taken can be merged into a single three-dimensional image. This single three-dimensional image can then be viewed in macro to look at the three-dimensional image, or more usually, in a sliced or sectioned configuration to look at the tissue in a particular plane of the tissue.

[0072] When the ultrasound device has performed its task and taken all the shots it is going to take with all of the arrays 60-70 and all of the elements being moved, the device will have collected enough data to assemble a three-dimensional view of the tissue sample. This three-dimensional view of the device is assembled by the software that compiles the various images taken by the ultrasound device and correlates them to

the tissue areas that they represent so that the software can determine which particular pixels of information correspond to which portion of the three-dimensional tissue sample.

[0073] Once this three-dimensional image is assembled, the next step is for the radiologist to review the image in order to make a diagnosis of the tissue from the image. One advantage of the present invention is that the data that is obtained can be manipulated to give the user almost an infinite number of two-dimensional and three-dimensional views of the three-dimensional tissue sample.

[0074] As discussed above, the large number of images taken by the large arrays of elements 200 can be compiled by the software 415C so that image information exists for each "point in three-dimensional space" within the tissue sample. Once image information is known for each point in space of the tissue sample, the image of the tissue can then be manipulated to provide the interpreting physician with any one of a virtually unlimited number of "views" of the tissue. The radiologist can then review one or a plurality of different views, as she believes necessary, in order to perform an appropriate review, and make a proper diagnosis.

[0075] In some situations, the radiologist will choose to review a three-dimensional view of the body tissue.

[0076] In many situations, the three-dimensional view that the device produces is not the only view that contains necessary diagnostic information, but will be viewed in conjunction with other "two dimensional" views. For example, a three-dimensional view of a finger would likely yield a view that appeared be similar to an exterior view of the finger. Similarly, a three dimensional view of a breast sample would likely have an appearance that was generally similar to an exterior view of the breast B.

[0077] However, a primary purpose of the ultrasound device is to enable the practitioner to view the interior of the tissue to determine the condition of the interior tissue of the breast or finger or other tissue sample, as that is where the cells of interest, such as the cancer cells are likely to reside. In order to see the interior of the tissue sample, it is preferred to obtain a thin section view, similar to a thin section view that one might obtain by thin slicing the tissue of the tissue sample. However, because of the plurality of images taken, the present invention enables the practitioner to view a wide array and variety of virtual thin sections of the tumor of interest.

[0078] Since the ultrasound device of the present invention is able to obtain information for, in theory, every point in space of the three-dimensional tissue object of interest the data can be manipulated to create an image of any one or more of these pixels of information or any grouping of these pixels. It is believed that the best way to create views that are useful to the practitioner is to create a thin section view, and preferably a plurality of this section view.

[0079] As shown in FIG. 13, the software provides the user with a three-dimensional image, and a pair of virtual cutting planes. The user can place the virtual cutting planes, such as virtual plane A and virtual plane B, in the orientation that the user prefers, and then look at a thin section is taken along that particular cutting plane. As is shown in the drawing, plane A is a plane that is disposed perpendicularly to plane B. It is important to note that since information exists for every pixel, for every point in space within the tissue, information can be gained from a plane at any angle. Although planes A and B are shown as perpendicular virtually and horizontally oriented planes, it will be appreciated that virtual planes A and B could

be oblique planes which for example could be oriented 10° or 20° to horizontal; or could be “tilted”. One could rotate plane A or B about any axis to achieve another plane, and could by looking at the information contained in a thin section taken along that plane, get the information that one would find by doing a section of the tissue sample along that plane.

[0080] Normally, when viewing a new tissue sample, the first thing that the practitioner, would do, is to take a quick “fly by” view of a tissue sample. In practice, this would likely represent, for example, the user taking a “nipple to thoracic bone” view of the breast, by looking at a plurality of slices that were cut through planes similar to plane A shown in FIG. 13, where the first plane that was shown is a plane that is parallel to the chest and that passes through the nipple, and the final plane section is a plane that is parallel to the chest and that is cut through the tissue in a position adjacent to the thoracic bone.

[0081] The doctor then uses this “fly by” to find the location of the tumor or cyst (if one exists) or tissue body of interest. Once the practitioner finds the tissue body of interest, he can choose to then look at this tissue body of interest from several different sections, such as section taken along a plane parallel to plane B, and also possibly, a view taken in a plane that is perpendicular to both planes A and B, and possibly other planes. By creating a sufficient amount of thin tissue sample images, wherein the images are taken along a variety of different planes, the user and the software can reconstruct a virtual three-dimensional image of the tumor or cyst of interest. Through this three-dimensional image, the user and diagnostician would be able to gain a better appreciation of the location of the tumor, the shape of the tumor, and the size of the tumor. Through these three items of information, one can gain a better understanding and appreciation of the nature of the tumor and its severity. Additionally, if temporally spaced sequential ultrasounds were taken of the tissue body of interest over time, one would be able to measure the growth and determine the growth rate (or lack of growth) of the tumor to better determine the aggressiveness of the growth of the tumor.

[0082] The biopsy procedure is also enhanced by the present invention’s capability of precisely locating the tumor in three-dimensional space. A biopsy is normally conducted by a very thin needle being inserted into the tissue of interest, and the tissue of interest being sucked out or otherwise retracted by the biopsy needle. The removed biopsy tissue is then tested through various diagnostic procedures to determine the nature of the tissue removed. Often, in the case of a tumor, the determination involves determining whether the tumor is benign or cancerous.

[0083] One difficulty that occurs when performing a biopsy is determining the precise location of the tissue of interest. By using the present invention, the practitioner has a better image of the tumorous tissue, and better location data relating to the three-dimensional positioning of tumorous tissue, since the present invention provides the practitioner with a three-dimensional map of both the “organ” (e.g. breast, pancreas, etc.) and also the potentially tumorous tissue within the “organ”.

[0084] Additionally, if the ultrasound device of the present invention is used simultaneously with the insertion of the biopsy needle, the ultrasound image information provided by the present invention would be real-time information. Since the information is delivered in real time, one can view the ultrasound image of a tissue of interest as the biopsy needle is

inserted into the organ, to ensure that the biopsy needle becomes inserted within the tumorous tissue to insure that the biopsy needle is in fact removing the desired tumorous tissue, rather than tissue outside of the body of interest.

[0085] Turning now to FIG. 6 and 6A, another type of probe 90 is shown. Probe 98 is the type that one might use for a prostate exam. Since the prostate probe 98 is being used internally and in this case, intra-rectally, size and shape constraints imposed by the need to insert the probe intra-rectally create significant design restraints that impact the size and shape of the probe. As one can imagine, a probe as large as one might use on the breast can not comfortably be used when the probe is being inserted internally.

[0086] It is envisioned that such a probe 98 will include head 100, a shaft 104 both of which are insertable in the rectum. The probe 98 also includes a handle 106 that is disposed externally during an examination. The practitioner uses the handle 106 to manipulate the probe 98 and more importantly, the probe head 100 within the colon. The probe head 100 preferably has a concave shaped wall engaging surface 106 that may be shaped similarly to a table spoon head. This concave surface 106 is placeable against the wall of the rectum adjacent to the prostate, so that the prostate can rest within the concave scoop surface 106. On the backside of the concave surface 106 is the array 108 of ultrasound elements 110, which in this case is probably a 3×3 array of ultrasound elements 110. Ultrasound elements 110 are preferably miniaturized versions of the elements shown in FIGS. 8-10. A communication chord 107 or radio transmitter (not shown) is provided to enable the probe 98 to communicate with CPU 400.

[0087] In order to operate this device, the ultrasound probe 98 is coupled to the CPU 400, and both are powered up. The probe 98 is then inserted through the patient’s anus and into the interior of the patient’s colon, with handle 106 being held externally and used to manipulate the probe head 100 into a position wherein the concave scoop surface 106 is positioned against a wall of the colon at a position adjacent to the patient’s prostate. When the probe head 100 is positioned properly, the driver software 4153 (FIG. 12A) will then be instructed to cause the 3×3 array 108 of ultrasound elements 110 to take images while the elements 110 move along their X axis and their Y axis. The images then taken will be transmitted to the computer 400 where they will be processed by the image processing software 415C so that a three-dimensional view of the prostate will be constructed. The three-dimensional view that is obtained from the array 108 of ultrasound elements 110 of the probe 98 will be constructed by a method analogous to the manner in which a three-dimensional image is constructed by your eyes through this through stereoscopic vision. When an image is “shot” from two different sensors that are spaced far enough apart, the images are merged three-dimensional information about the object of interest can be obtained.

[0088] Once the ultrasonically captures a three dimensional image of the prostate, the image will then be analyzed by the urologist (or pathologist or radiologist) in much the way that the breast was analyzed. In particular, the imaging software 415C will be employed to create a plurality of thin section images constructed along a variety of different planes to thereby provide a plurality of virtual thin sections taken from a plurality of angles. As also with the breast procedure described above, the imaging software can be employed to create a three dimensional image of the prostate by having the

cut plates, so that the radiologist can view a variety of virtual thin section images or views of the prostate.

[0089] Turning now to FIGS. 8-10 the construction of three alternate embodiment elements 200, 37, 300 is discussed. The embodiments include cylindrical element 200 shown in FIG. 8; the long rectangular cuboid element 37 shown in FIG. 9; and the short rectangular cuboid element 300 shown in FIG. 10.

[0090] Turning first to FIG. 8, the cylindrical element 200 includes a piezoelectric crystal 210, which comprise a 4 mm×4 mm element 210 that is disposed at one end of the element 200. The element 200 is shown as having a generally cylindrical configuration and includes a body portion comprising an exterior housing 202, and a first or "head" end 204, and a second or "base" end 206. The piezoelectric crystal 210 is disposed at the head end 204. The housing 202 includes a circular collar portion 212 disposed adjacent to the head end 204, whose purpose is to help couple the piezoelectric element 200 onto the array base 388 (FIG. 11).

[0091] It will be appreciated that although the housing 202, generally encloses all of the internal components, the view shown in FIG. 8 comprises a cut-away view so that the internal components can be explained and understood by the reader. The housing 202 generally extends between the collar 212 and the second end 206. It will be noted that the base end portion 212A of the housing is configured into a base for receiving the wires for driving the piezoelectric element 210, and for serving as a base onto which the internal components can be mounted.

[0092] A piezoelectric motor is provided for moving the piezoelectric crystal element 210 along its X and Y axis in four degrees of freedom. The motor assembly includes a longitudinal member 220 and a circular motor member 230. The longitudinal member 220 includes a proximal end 218 disposed relatively closer to the base end 206, and a distal end 214, disposed relatively closer to the head end 204. The distal end 214 is coupled onto the sides of the piezoelectric crystal 210, in a manner generally similar to that shown in connection with FIGS. 1-3C.

[0093] The longitudinal member 220 also includes an intermediate portion, that consists of two axially extending metal bands 222, 224. The axially extending bands 222, 224 are capable of expanding or contracting in an axial direction. Through this axial expansion and contraction, the axially extending band 222, 224 can move the piezoelectric crystal 210.

[0094] The proximal end 218 of the longitudinal member 220 includes a coupling for coupling the proximal end 218 of the longitudinal member 220 to the circular member 230. The circular member 230 is disposed in a generally radially extending plane, that is generally perpendicular to the axis of the longitudinal member 220. The circular member 230 extends radially outwardly, and has an axis that extends generally co-linearly with the axis of the element 200.

[0095] The element 200 also includes a pair of lateral stabilizers 250, 260. The lateral stabilizers 250, 260 do not necessarily perform any role within the transmission and reception of ultrasound waves, or the movement of the piezoelectric crystal 210. Rather, they help to stabilize the device and provide couplers and attachment points for maintaining the internal components within the element 200.

[0096] A central shaft element 270, is operatively coupled to a Y axis mover 240. The Y axis mover 240 has segments 242, that are coupled to the side of the piezoelectric crystal

210. Segments 242 move the piezoelectric crystal 210 about its Y axis, as compared to member 214 that moves the piezoelectric crystal 210 about its X axis.

[0097] Wires (not shown) are provided for providing electrical signals to the various components, such as the band 220 and the Y mover 240, to cause these bands 220, 240 to expand and contract, and thereby move the piezoelectric crystal 210.

[0098] Your attention is now directed to FIG. 9. FIG. 9 shows a rectangular cuboid-shaped ultrasound element 37. Rectangular cuboid-shaped element 37 includes a housing 39 that includes a base end 58, and a head end 59. A moveable piezoelectric crystal 30 is disposed at the head end, similar to piezoelectric crystal 210 of FIG. 8.

[0099] An X axis moveable band is provided that includes a first segment 38 and a second segment 43.

[0100] The first mover 31 includes a first segment 38 and a second segment 43. The first end 40 of the first mover 31 is coupled to the body portion 40, and the second end 41 of the mover 31 is coupled to the side edge portion 47 of the piezoelectric crystal 30. Similarly, the first end 150 of the second mover 142 is coupled to the body portion 39, and the second end 153 is coupled to a second side edge portion 155 of the piezoelectric crystal 30.

[0101] A current is applied to second segment 43 that causes the second segment 43 to either expand or contract. First segment 38 does not necessarily expand or contract, but rather serves as an extender that moves in response to the expansion or contraction of second segment 43. Segment 38 of the X movable band is coupled to the side surface 47 of the piezoelectric crystal 30 to move the piezoelectric crystal about the X axis.

[0102] Similarly, a Y moveable band 142 is provided that is coupled at its 142 distal end to a side edge of the piezoelectric crystal 30. A signal is applied to band 142 to enable it to expand or contract, to thereby move the piezoelectric crystal about a Y axis. The proximal (first) end 150 of the moveable band 142 is coupled to either another band extender (not shown) or to a base member. Additionally, a base end member 40 is disposed at the proximal end of the element 37.

[0103] A shortened rectangular cuboid element 300 is shown in FIG. 10. Shortened element 300 also includes an X moveable band 338, and a Y moveable band 342. Generally, shortened rectangular cuboid element 300 is constructed similarly to, but shorter than the elongated rectangular cuboid element 37 shown in FIG. 9.

[0104] Finally, turning now to FIG. 11, an array of elements 200 is shown. The array of elements 200 are coupled onto a frame 388. Frame 388 is generally stationarily positioned. Each of the elements 200 is individually moveable with respect to the frame 388. Preferably, the elements 200 move simultaneously and synchronously, because such movement helps to reduce the processing burden placed upon the central processing unit 400 that is processing the images captured by the piezoelectric crystals 390 of the array 198 of element 200.

[0105] In the foregoing description relating to the elements 200, it will be appreciated that generally, the barrel portions of the elements 200 remain fixedly positioned with respect to the frame 388, with the only moving member of the elements 200 being the piezoelectric crystals 390, that can move along X and Y axes in four degrees of freedom by the piezoelectric motor. It will be noted that the elements 200 shown in FIG. 11 are constructed similarly to element 200 shown in FIG. 8. However, it will also be appreciated that the elements 37, 300

shown in FIGS. 9 and 10, respectively, could be substituted for the generally cylindrical elements 200 shown in FIG. 11. [0106] To improve over the existing ultrasound techniques and in an attempt to gain a three-dimensional image, the Applicant has invented an alternate embodiment automated ultrasound system 500 shown in FIGS. 14-17 that is particularly useful for disposing pathologies in tissues of interest that are capable of being placed in a receiving cup, such as breast, penis, testicular, hand and feet tissue. In the description hereunder, an embodiment will be described that is particularly useful for diagnosing breast pathologies. In this alternate embodiment, automated breast ultrasound system, a linear array of ultrasound elements 600 (FIG. 15) are placed on a base member 602 that is part of a rotatable platform portion 501. The rotatable platform portion 501 is moveable by a motor 508 so that the entire platform 501 and the array 600 of the ultrasound elements 600 rotate about the axis of the receiving cup 606 as the platform 501 rotates about the axis of the receiving cup. The ultrasound elements 600 can be similar to the elements (e.g. 37) shown in FIGS. 8-10, except that the elements 600 need not include moveable piezoelectric crystals 30, 210.

[0107] The device 500 includes a water filled cup 606. The patient places her breast into the interior 608 of this water-filled cup 606, and the platform 501 containing the ultrasound transducer 600 is rotated around the plantar-dorsal axis PDA of the breast B in the cup 606 interior 608 in a controlled manner so that the transducer 600 captures images of the breast B from 360 degrees about the plantar-dorsal axis PDA of the breast B. These 360 degree images are then processed by image processing software so that the user can examine the sequential two dimensional images to determine whether any abnormal features exist or occur within the breast.

[0108] Additionally, the software has features that enable the practitioner to manipulate the image. In manipulating the image the user can create virtual "thin slices" of the breast tissue to enable the interpreting physician to view a virtual sliced section from any angle of the 360 degrees, because in this 360 degree process, the device obtains a graphic representation of every pixel corresponding to every point in three-dimensional space within the breast B. By knowing where those points in space are located; and by knowing what those points of space look like for every point within the breast, the information so obtained can be manipulated to create a view or image of any point or section of the breast from any angle to get different views of the possible abnormal cells, or array of cells within the breast.

[0109] A movable platform ultrasound 500 that is shown in FIGS. 14 and 17 includes a rotatable platform portion 501, that is mounted above a stationarily positioned bracket 502. Bracket 502 is preferably made from an aluminum material, and is generally C-shaped. The bracket 502 is coupled to an examination table member, such as member 504. Although member 504 need not be part of the examination table, normally, it is a portion of the table that is disposed under the examination table top surface 632 (FIG. 16).

[0110] A motor 508 is positioned underneath the bracket 502, and includes a power cord 501 for preferably providing alternating current power to the motor 508 to cause the motor to rotate. Because the device is capable of rotating both clockwise and counterclockwise, the motor should be designed to either rotate in both directions, or else, be coupled to or contain some transmission mechanism that permits the motor to rotate in both a clockwise and a counterclockwise direc-

tion. The motor 508 includes an output shaft/worm receiving collar 514. The output shaft/worm receiving collar 514 preferably includes a threaded interior surface for receiving the threaded exterior surface 516 of worm 515, which preferably is screw-like and contains a spirally threaded exterior surface.

[0111] A stop sensor 518 is fixedly coupled to the exterior surface of the bracket 502, and was provided for sensing the position of a pendulum member 520. Stop sensor 518 is coupled to the motor 508 for turning the motor on and off, in response to the rotation position of the platform portion 501, as interpreted, through the position of the pendulum member 520.

[0112] Pendulum member 520 is pivotably coupled to the bracket 502 by a pivot member 522. The pendulum member 520 includes an upper surface 524 that is coupled to the disc-shaped base member 536 of the rotatable platform portion 501. The pendulum member 520 also includes a lower surface 528, that is operatively coupled to the sensor member 518. The pendulum and sensor also cooperate to aid in the axial movement of the base member 618. The pendulum member 520 is operatively coupled to the sensor member 518 so that the pendulum 520 when so actuated, can cause the rotation of the rotatable portion 501 to cease relative to the rotation of the worm 515. By stopping the rotation of rotatable member 501, the relative movement between the worm 515 and the rotatable member 501 is allowed to occur. This allows the worm 515 to either extend axially to thereby reduce the size or the volume of the interior 608 of the cup 606; or alternately, to move axially in a retracting direction to increase the volume of the cup 606. As will be appreciated, as the effective length of the worm 515 decreases, the volume of the cup 606 will increase; and, conversely, as the relative length of the worm 515 increases (as a longer length of the worm 515 becomes disengaged from the worm receiving collar 538), the base member 608 of the cup 606 will move axially outwardly to reduce the effective volume of the interior 608 of cup 606, and thereby place the ultrasonic linear array 600 closer to the table surface 632 (FIG. 15).

[0113] The rotatable portion 501 includes a disc-shaped base plate 536, having a central aperture 538, through which the output shaft/worm receiving collar 514 can pass. The rotatable portion 501 also includes a first standing member 542, a second standing member 544 and a third standing member 546. The first, second and third standing members 542, 544, 546 are spaced from each other, so that the center lines in each of the three standing members 542, 544, 546 are disposed approximately 120° apart.

[0114] The standing members 542, 544, 546 couple together the base plate 536, with the cup portion 606 of the rotatable portion 501. The cup 606 is shown as including an interior 608. As ultrasound uses the passage of sound waves through preferably an aqueous medium, the cup 606 is designed so that the interior 608 can be filled with a fluid such as water, along with being filled with the tissue of interest, such as the breast B shown in FIGS. 16 and 17.

[0115] The volume of the interior 608 of the cup is variable, so that the volume can be decreased relatively when one is working with a relatively smaller tissue sample, such as the rather smaller breast shown in FIG. 16. The volume interior 608 of the cup 606 can also be increased to accommodate a larger tissue sample, such as the relatively larger breast B shown in FIG. 17. This changing volume occurs through the axial movement of the base member of the cup, that defines the upper surface 620 of the base of the cup.

[0116] The cup portion 606 includes a cylindrical side wall 612, a disc-shaped exterior base member 616, and a disc-shaped interior base member 618. The interior and exterior base members 616, 618 are axially movable within the cylindrical side wall 612 due to the action of threaded 516 (worm) 515. As shown in FIG. 16, the screw 515 can move the base members 616, 618 to a relatively axially outwardly position to thereby form a relatively reduced volume cup interior 608. When this occurs, the linear array of ultrasound transducers 600 that are placed on the angled base 602 will be placed relatively closer to a smaller tissue sample, such as the smaller breast B that is shown in FIG. 15.

[0117] Similarly (as shown in FIG. 17), the threaded 511 worm 515 can cause the axial movement of the disc-shaped exterior 616 and interior 618 base members, to cause the base members to move axially outwardly, to thereby create a relatively larger volume within the interior 608 of cup 606. This relatively larger volume is provided for accepting the relatively larger tissue sample of relatively larger breast B, to accommodate the additional space requirements required by larger breast B. When so done, preferably the linear array of ultrasonic transducer 600 that are placed on ramp 602 are positioned close to and adjacent to the tissue of the breast B.

[0118] As the Applicant's have found that better results are achieved when the array of ultrasonic transducers 600 are placed relatively closer to the breast tissue, the axially movable platform 616, 618 of the present invention, by enabling the ultrasonic transducer 600 be positioned close to the breast tissue, is believed to have better performance characteristics over a wider range of conditions than, for example, a fixedly positioned ultrasonic transducer 602. It is understood that in order to accommodate tissues of different sizes, a fixedly positioned ultrasonic transducer would likely need to be in a position closer to that shown in FIG. 17, so that it would provide enough volume in the interior 608 of the cup to accommodate the larger breast B. Although a fixed volume and position ultrasonic device 600 would likely work well when performing a procedure on a larger breast such as breast B shown in FIG. 17, the rather significant distance between the ultrasonic transducer array 600 and a smaller breast B would be sufficiently great, so as to likely significantly degrade the quality of the image taken by the ultrasonic transducer array 600 when used with a smaller breast.

[0119] The cylindrical wall 612 includes an exterior surface 622 and an interior surface 624. Preferably, a water tight seal exists between the radially outward edges of the base member 616, 618 and the interior surface 624 of the cylindrical wall 612. This water tight seal can be achieved through the use of an elastomeric material, such as an elastomeric o-ring or the like.

[0120] Cup 606 also includes an axially outwardly positioned, radially outwardly extending flange portion 630. Flange portion 630 is generally annular, and extends radially outwardly, and provides a surface for coupling the cup member 606 to an examination table top 632. Preferably, the radially outwardly extending flange portion 630 and the examination table top 632 should be relatively co-planar. Additionally, the flange should have an outer diameter that is greater than the general diameter of the exterior surface 622 of the cup 606 or the upstanding members 542, 544 which surround the cup 606. For Example, the diameter of the cup 606 is about 6 inches (15.24 cm), whereas the diameter of the flange is between about 15 and 18 inches (38.1 and 45.72 cm).

[0121] A drain 636 is placed in the base member 616, 618 to extend there through, and includes a plug, or valve, that permits the user to selectively permit and prevent the flow of fluid through the drain 636, 638. As water is preferably placed within the cup 606 during a procedure, a means should be provided for draining water from the interior of the cup 608. Preferably, the water is changed in between patients, but in any event, there should be a means for withdrawing water.

[0122] In the instant invention, the drain 636 is coupled to a drain hose 638 that can lead to either a water catching receptacle or a drain. A power cord 642 is designed to preferably extend through the base member 616, 618 to provide the power and communication signals between the CPU 400, and the ultrasonic array 600.

[0123] In operation, one desiring to use the ultrasound device shown in FIG. 16 should have the patient lay face down upon a table top 632, and insert the tissue of interest (here shown as a breast) into the interior 608 of cup 606. The worm 515 is then rotated relative to the cup portion 601, so that the platforms 618, 616 are moved into their appropriate axial position so that the cup 606 has sufficient volume to receive the tissue of interest, while still placing the ultrasonic transducer array 600 close to the breast, as shown in each of FIGS. 16 and 17.

[0124] Preferably, water is inserted into the interior of the cup before the breast is inserted therein but may be inserted after insertion of the breast.

[0125] The device is then powered up and turned on. The ultrasonic transducer 600 then takes a plurality of images, as the rotatable portion rotates the ultrasonic transducer array 600 relative to the breast B, about the plantar dorsal axis PDA of the breast B. The ultrasonic transducer 600 is rotated around the axis PDA until images are obtained from a 360° about the axis, PDA. Although pictures can be shot as the ultrasound moves continuously, it has been found by the Applicants that the device works well if the ultrasonic transducer moves among 20 different stop points separated by about 18°, so that images are taken from 20 positions about the 360° circumference of the axis PDA. As discussed above in connection with the moveable ultrasound element version of the device, the plurality of images taken by the linear array of ultrasonic transducers are then fed to the image processing portion of the software, so that the images can be processed into a plurality of different "views" for use by the interpreting physician.

[0126] Although the invention has been described with reference to certain preferred embodiments, it will be appreciated that variations and modifications exist within the scope and spirit of the invention.

What is claimed:

1. An ultrasound device for diagnosing pathologies in a tissue of interest comprising
 - a platform member
 - an array of at least two ultrasonic elements coupled to the platform member, each of the at least two elements including
 - a body portion
 - a piezoelectric crystal member having a first axis and a second axis
 - a first mover capable of moving the piezoelectric crystal member about the first axis of the crystal
 - a second mover capable of moving the piezoelectric crystal about the second axis of the crystal

a controller for causing the first mover and second mover to move the piezoelectric crystal about the respective first and second axes for enabling the ultrasound device to capture a plurality of images at different positions of rotation about the first and second axes.

2. The ultrasound device of claim 1 wherein the first and second axes of the piezoelectric crystal comprise respectively an X-axis and a Y-axis, and wherein the first mover is capable of moving the piezoelectric crystal about the X-axis, and the second mover is capable of moving the piezoelectric crystal about the Y-axis.

3. The ultrasound device of claim 1 further comprising imaging software for correlating the plurality of images to produce at least one of a thin section image and a three-dimensional image.

4. The ultrasound device of claim 3 wherein the imaging software is capable of correlating the plurality of images to produce a plurality of thin section images.

5. The ultrasound device of claim 4 wherein the plurality of the section images produced comprise a plurality of thin section images showing parallel planes of the tissue of interest.

6. The ultrasound device of claim 3 wherein the imaging software is capable of correlating a plurality of images to produce a plurality of views of the tissue of interest showing different aspects of the tissue of interest.

7. The ultrasound device of claim 3 wherein the imaging software is capable of correlating a plurality of images of a tissue sample to create a three-dimensional view of a tissue of interest within the tissue sample.

8. The ultrasound device of claim 1 wherein the first mover comprises a band comprised of a material capable of expanding and contracting under the influence of energy applied to the band, wherein the expansion and contraction of the material of the band moves the piezoelectric crystal about the first axis.

9. The ultrasound device of claim 9 wherein the band comprises a material band having a first end coupled to the body portion of the ultrasonic element and a second end coupled to a first edge portion of the piezoelectric crystal.

10. The ultrasound device of claim 9 wherein the second mover comprises a metal band capable of expanding and contracting under the influence of the application of energy to the band, where the expansion and contraction of the metal of the band moves the piezoelectric crystal about its second axis, and wherein the band includes a first end coupled to the body portion of the ultrasonic element and a second end coupled to a second edge portion of the piezoelectric crystal.

11. The ultrasound device of claim 1 further comprising a tissue receiving member, wherein the platform member is

fixedly coupled to the tissue receiving member and the body portions of the at least two elements are fixedly coupled to the platform member, and wherein the piezoelectric crystal members are movable relative to the platform and body portion.

12. The ultrasound device of claim 11 wherein the tissue receiving member comprises a cup member capable of receiving a media and the tissue of interest,

the cup comprising the platform member to which the array of at least two ultrasonic elements are coupled, and the array of at least two of ultrasonic elements comprises at least four arrays of at least two ultrasonic elements circumferentially arrayed around the cup to enable the ultrasonic elements to capture images fully around an axis of the tissue of interest.

13. The ultrasound device of claim 11 wherein the tissue receiving member comprises a head portion of a hand held instrument that also includes a handle portion, the head portion comprising the platform to which the array of at least two ultrasonic elements are attached.

14. The ultrasonic device of claim 13 wherein the head is sized and configured for insertion into a mammalian orifice for permitting the head portion to be positioned internally within the orifice and adjacent to an internally disposed tissue of interest.

15. An ultrasound device for diagnosing pathologies in a tissue of interest comprising a platform member, the platform member including a tissue receiving cup,

an array of at least two ultrasound elements positioned to obtain ultrasonic images of a tissue of interest disposed within the tissue receiving cup, the array being moveable about the tissue of interest for obtaining images of the tissue from a plurality of different positions, and an array mover capable of moving the array of ultrasound elements to change distance between the array and the tissue of interest and to change relative angular position between the array and the tissue of interest.

16. The ultrasound device of claim 15 wherein the array mover includes a rotational mover for changing the angular position of the array and tissue of interest by rotating the array about an axis of the tissue of interest.

17. The ultrasound device of claim 15 wherein the array mover includes a linear mover coupled to each of the cup and array for linearly moving the cup to both better position the array relative to the tissue of interest and to change a volume of an interior of the tissue receiving cup.

18. The ultrasound device of claim 17 wherein the array mover includes a motor member having an output shaft coupled to a worm, the worm being coupled to the cup to change the volume of the interior of the tissue receiving cup.

* * * * *

专利名称(译)	可移动的超声波元件，用于医疗诊断设备		
公开(公告)号	US20090259128A1	公开(公告)日	2009-10-15
申请号	US12/422766	申请日	2009-04-13
[标]申请(专利权)人(译)	斯特里布林点I		
申请(专利权)人(译)	斯特里布林点I		
当前申请(专利权)人(译)	斯特里布林点I		
[标]发明人	STRIBLING MARK L		
发明人	STRIBLING, MARK L.		
IPC分类号	A61B8/14		
CPC分类号	A61B8/0825 A61B8/12 A61B8/406 A61B8/4461 A61B8/4483 A61B8/445 A61B8/523 G01S7/5208 G01S15/8936 G01S15/8993 G10K11/352 A61B8/483		
优先权	61/124064 2008-04-14 US		
外部链接	Espacenet USPTO		

摘要(译)

根据本发明，提供了一种超声设备，用于诊断感兴趣组织中的病变。超声装置包括平台构件和耦合到平台构件的至少两个超声元件的阵列。所述至少两个元件中的每一个包括主体部分和压电晶体构件。压电晶体构件具有第一轴和第二轴。提供了一种能够使压电晶体构件绕晶体的第一轴移动的第一移动器。提供第二移动器，其能够使压电晶体围绕晶体的第二轴移动。提供一种控制器，用于使第一动子和第二动子围绕相应的第一和第二轴移动压电晶体，以使超声装置能够捕获围绕第一和第二轴的不同旋转位置的多个图像。

