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(12) **United States Patent**
Crowley et al.(10) **Patent No.:** **US 6,847,454 B2**(45) **Date of Patent:** **Jan. 25, 2005**(54) **SYSTEMS AND METHODS FOR
PROCESSING SIGNALS FROM AN
INTERFEROMETER BY AN ULTRASOUND
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(57)

ABSTRACT

An imaging system comprises an interferometer and an ultrasound console that processes signals from the interferometer into an image for display. The interferometer may include one or more multi-element photo detectors with a plurality of parallel outputs. A parallel to serial converter is provided between the parallel output of the interferometer and the input of the ultrasound console, to convert the signals provided on the parallel outputs into a serial signal for analysis by the ultrasound console. The interferometer may be selectively coupled to the ultrasound console and the system may further comprise an ultrasound device that may also be selectively coupled to the console, offering a user the option of using either the interferometer or the ultrasound device. The ultrasound console may also include two inputs, one for the interferometer and the other for the ultrasound device. The interferometer and the ultrasound device may both be carried by catheters for insertion into internal body cavities, such as blood vessels. Imaging methods are also disclosed.

41 Claims, 14 Drawing Sheets

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U.S.C. 154(b) by 192 days.(21) Appl. No.: **10/020,040**(22) Filed: **Oct. 18, 2001**(65) **Prior Publication Data**

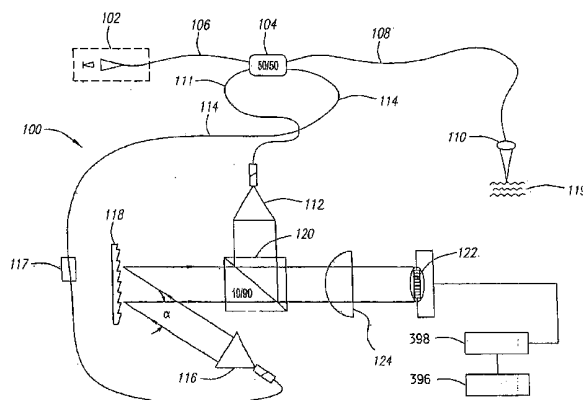
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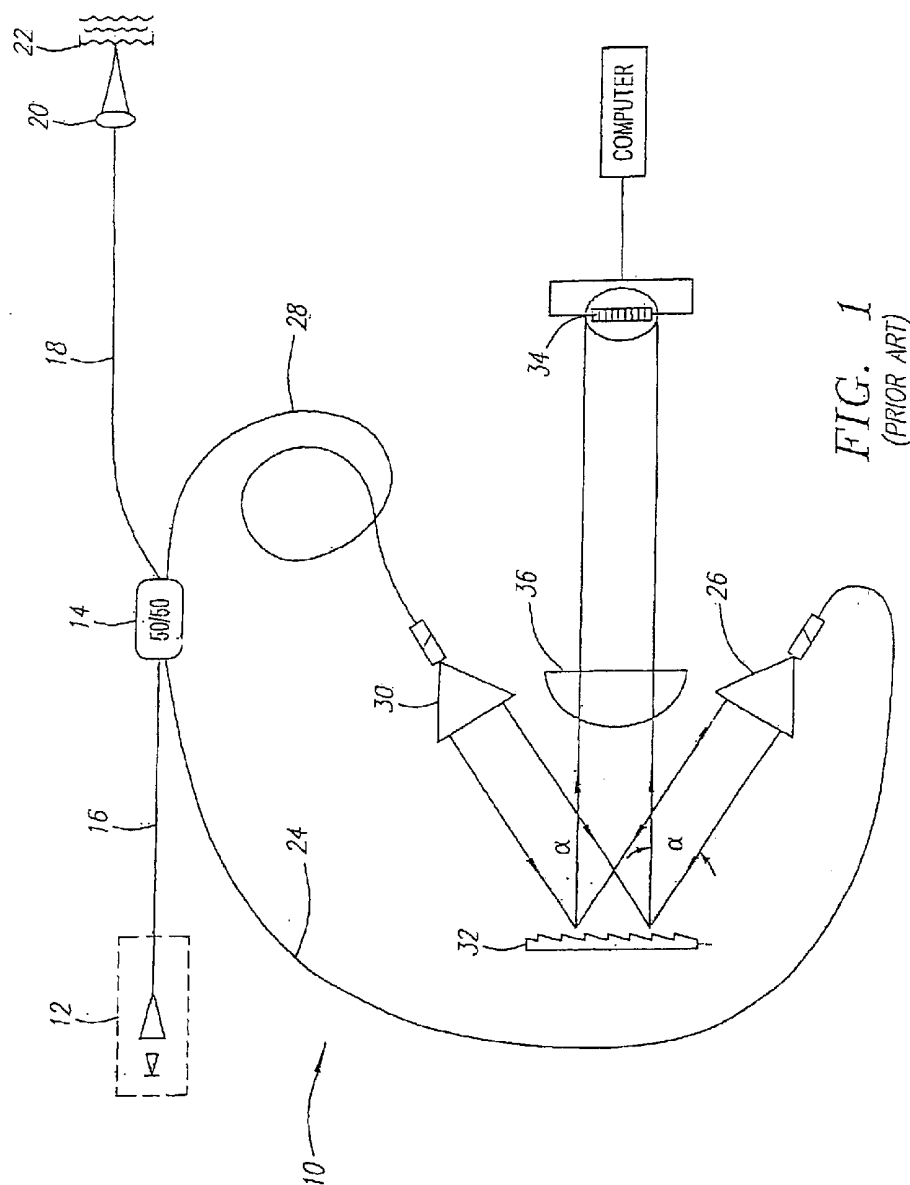
Related U.S. Application Data

(63) Continuation-in-part of application No. 09/909,357, filed on
Jul. 18, 2001, and a continuation-in-part of application No.
09/906,903, filed on Jul. 16, 2001, now Pat. No. 6,728,571.(51) Int. Cl.⁷ **G01B 9/02**(52) U.S. Cl. **356/479; 356/497; 356/502;**
73/657(58) Field of Search 356/497, 521,
356/502, 479, 492, 495; 73/655, 657(56) **References Cited**

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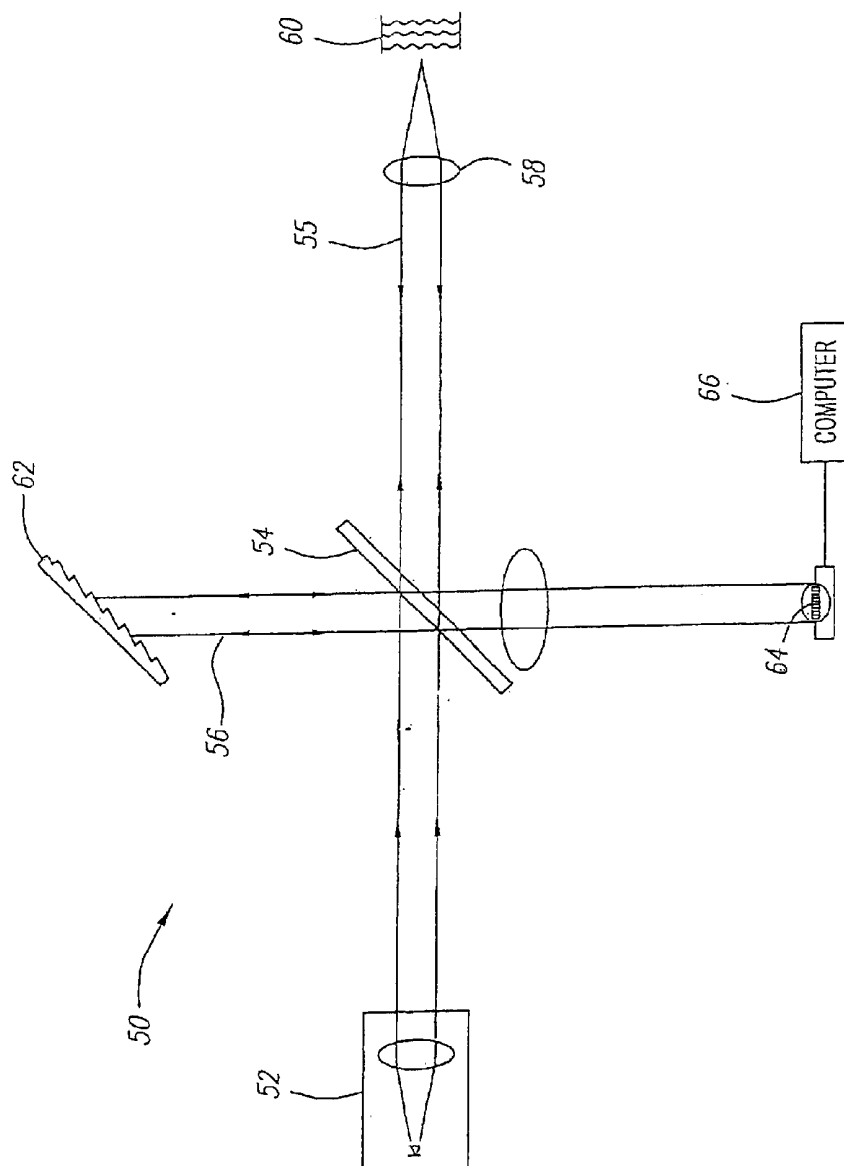


FIG. 2
(PRIOR ART)

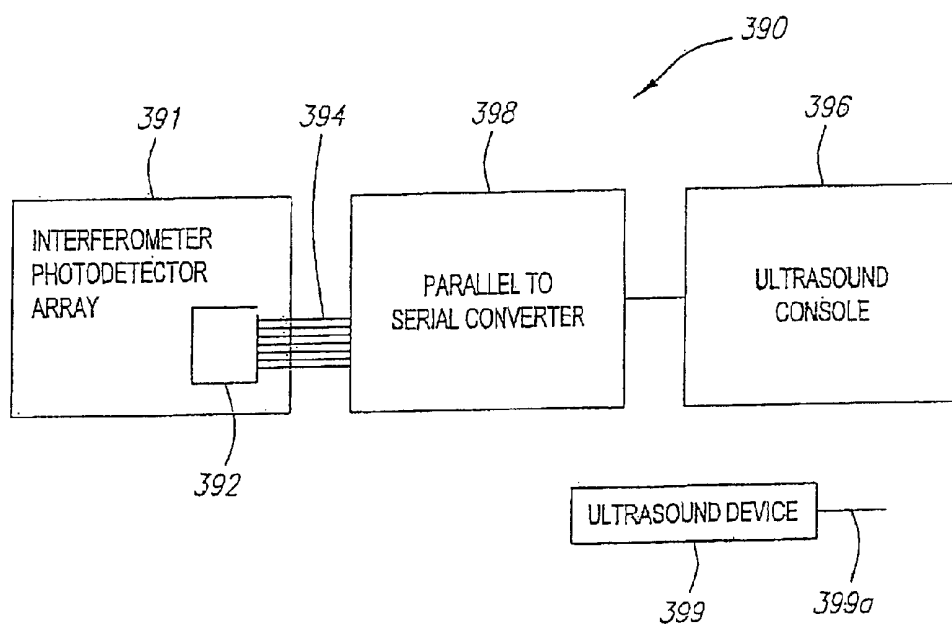


FIG. 3

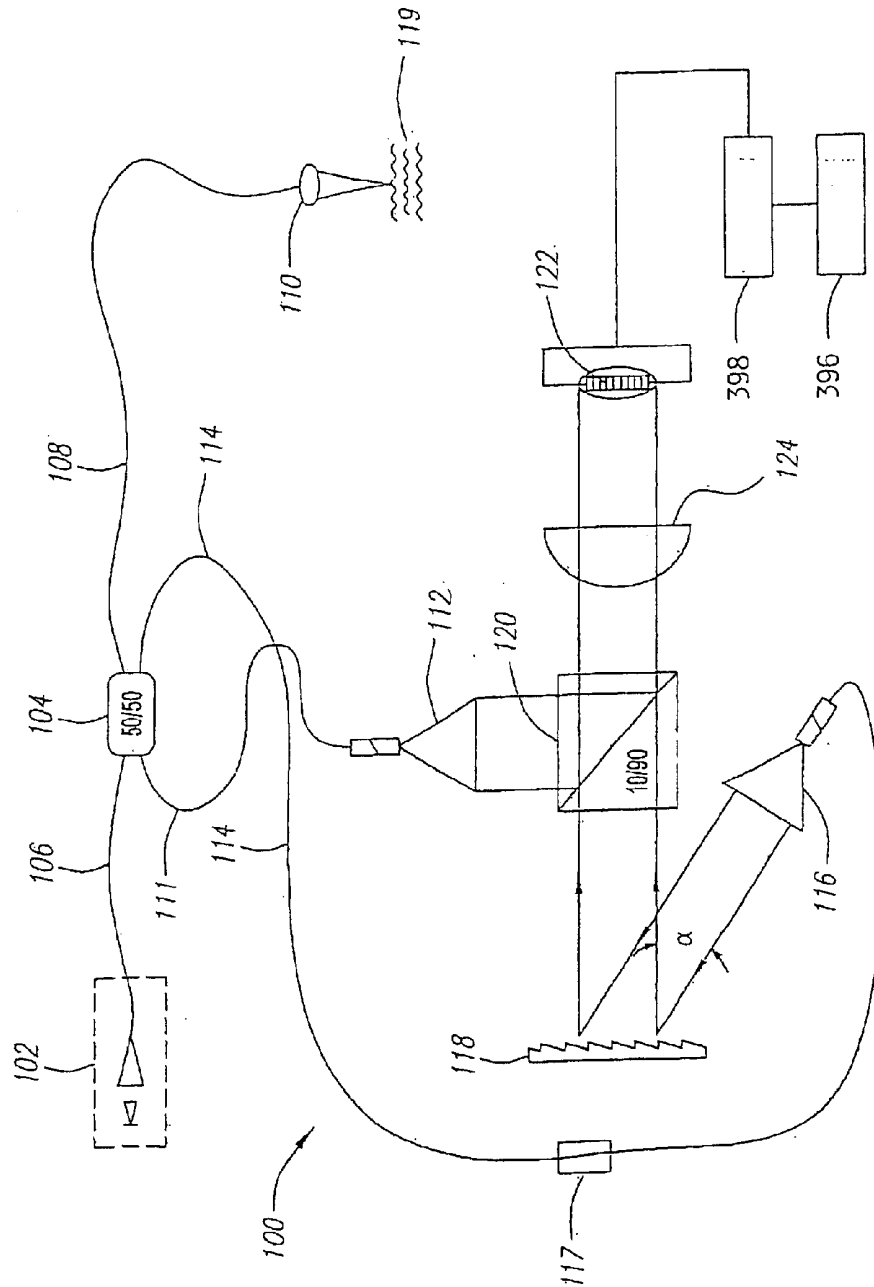


FIG. 4A

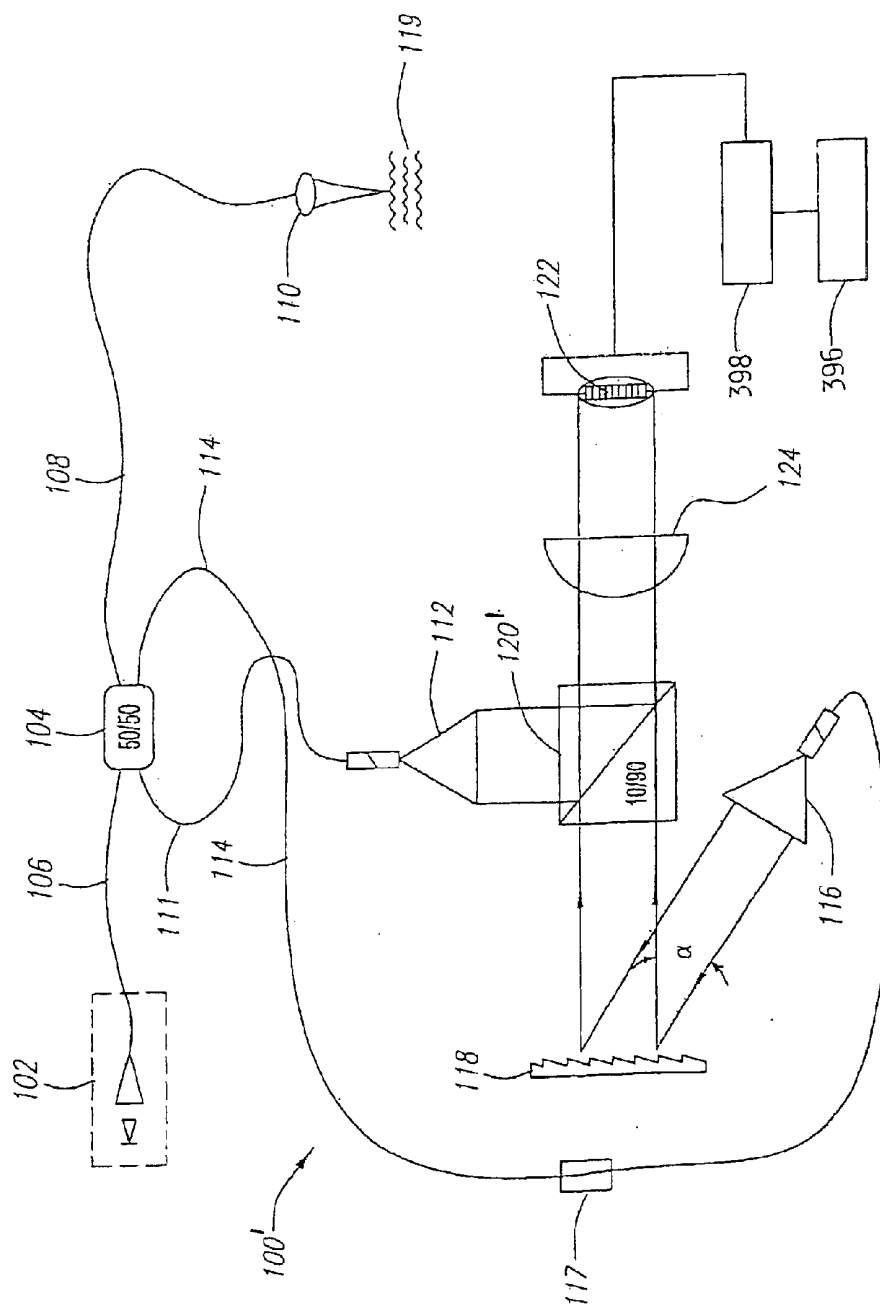


FIG. 4B

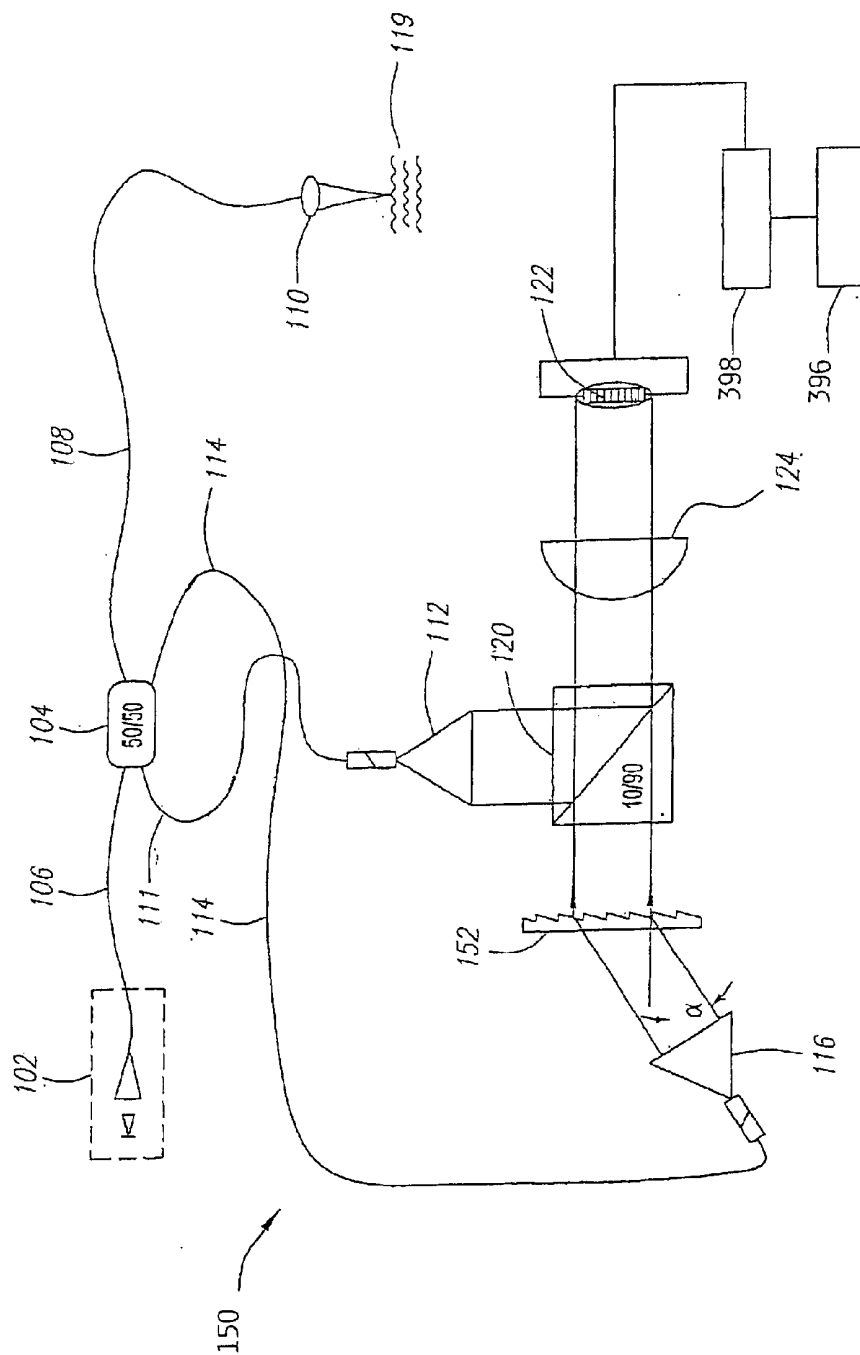


FIG. 5

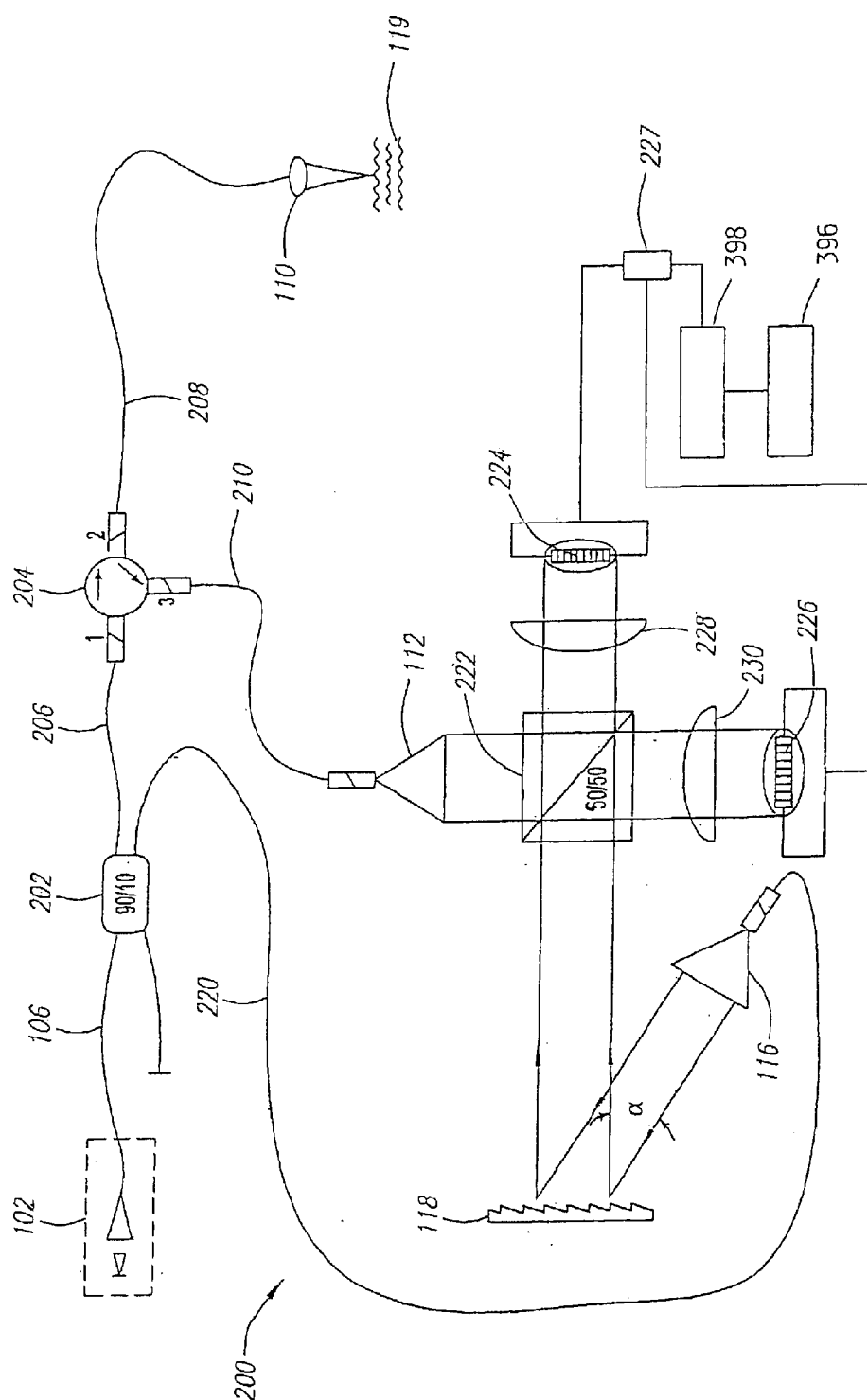


FIG. 6

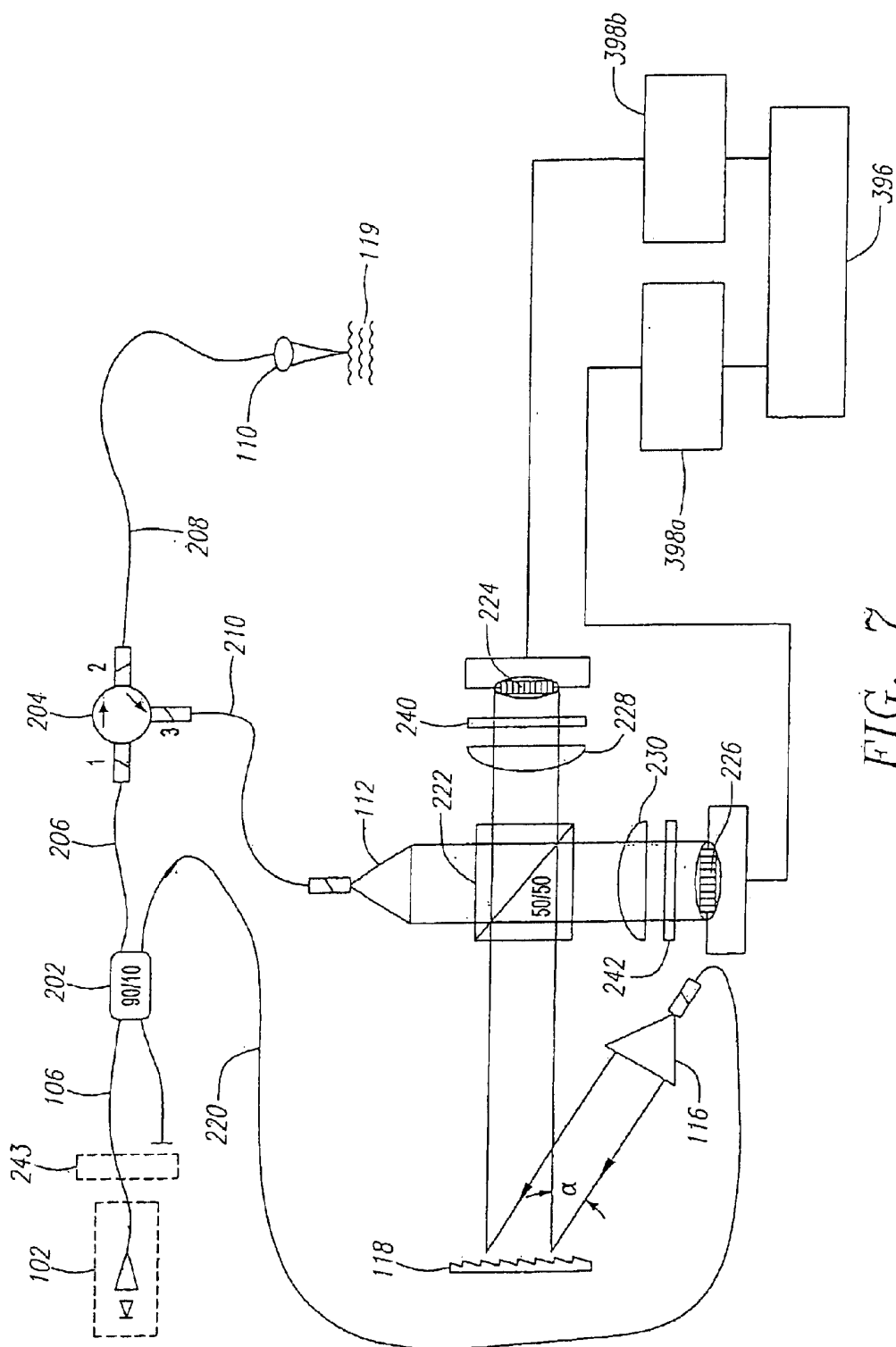
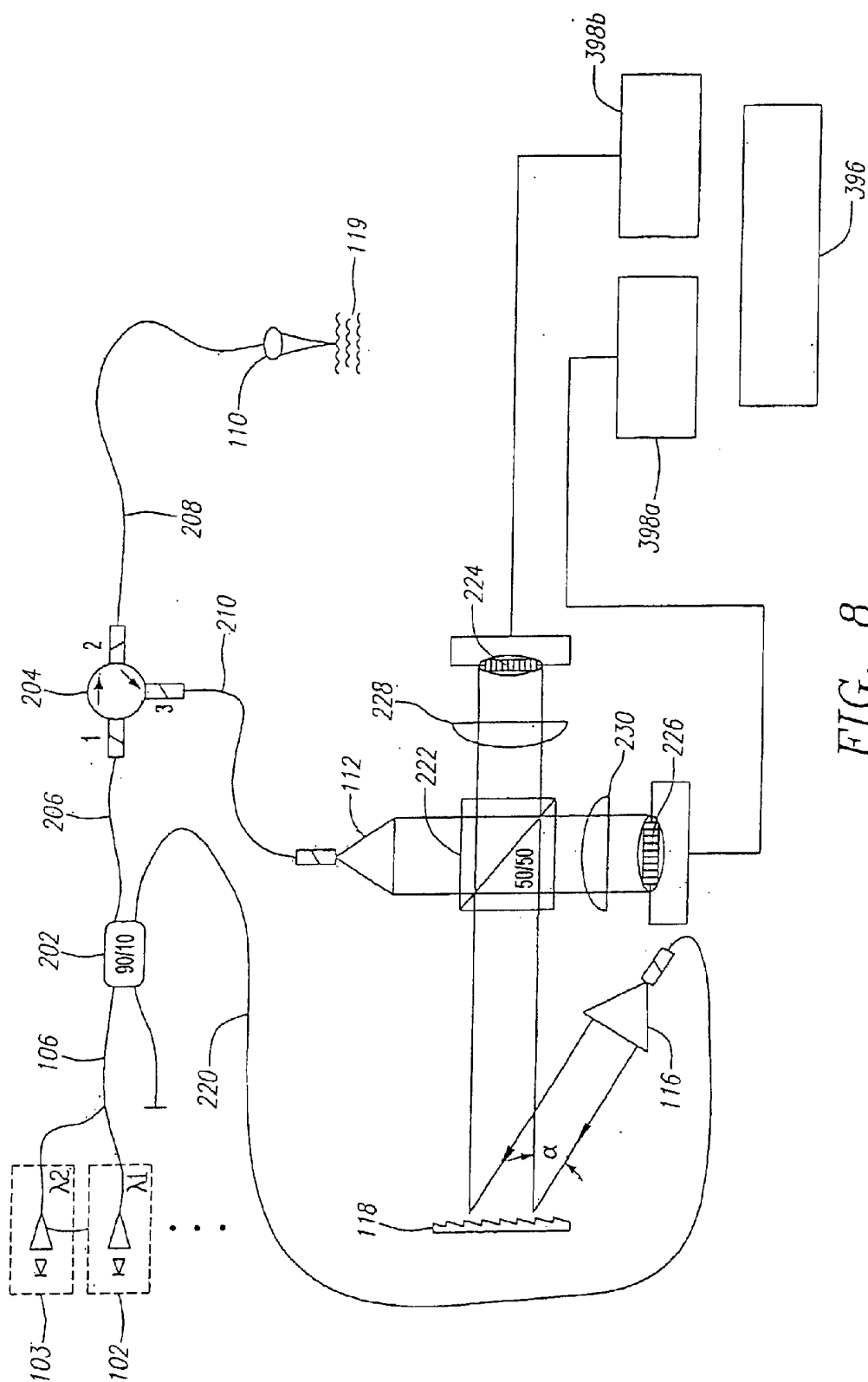


FIG. 7



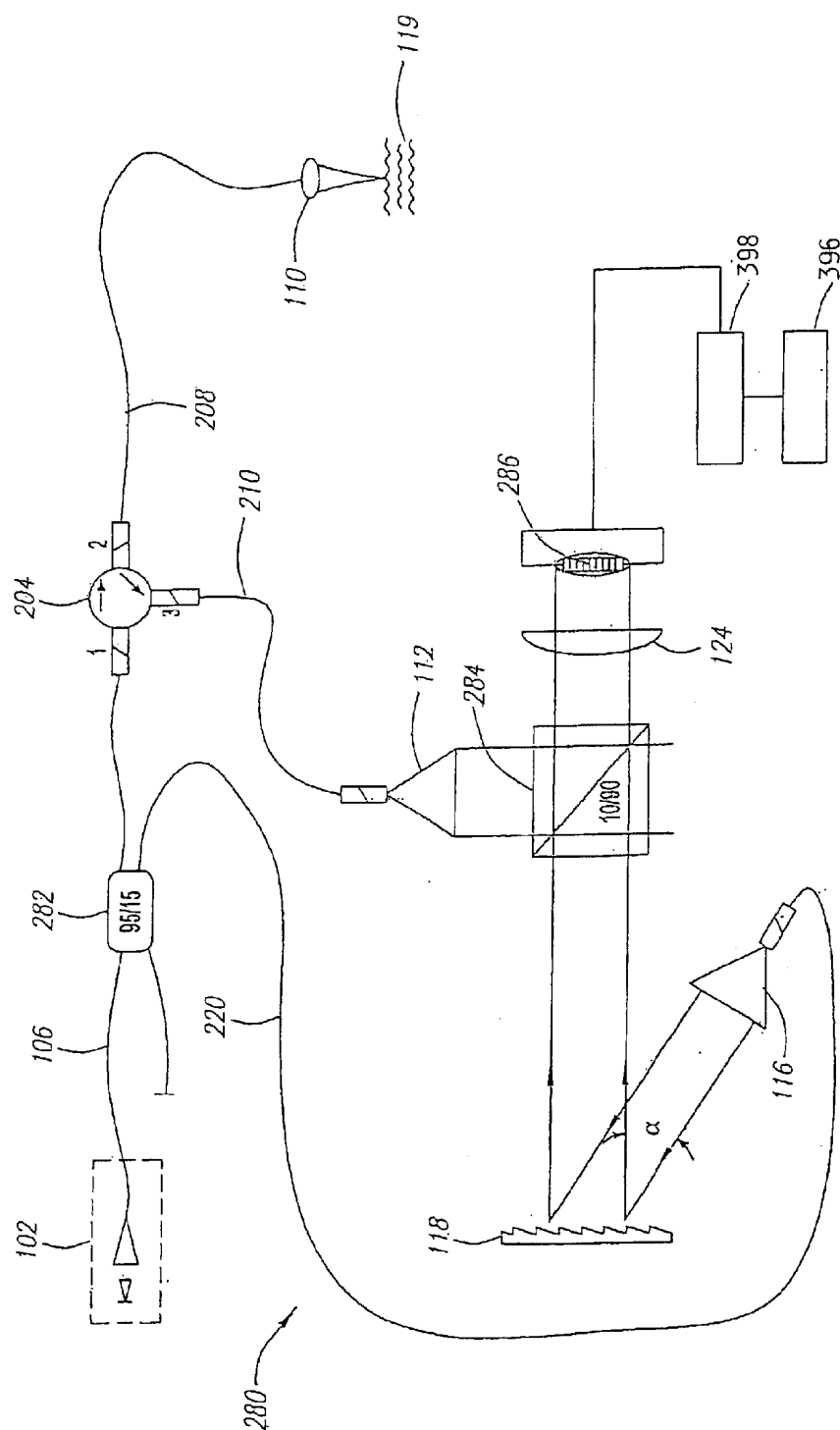


FIG. 9

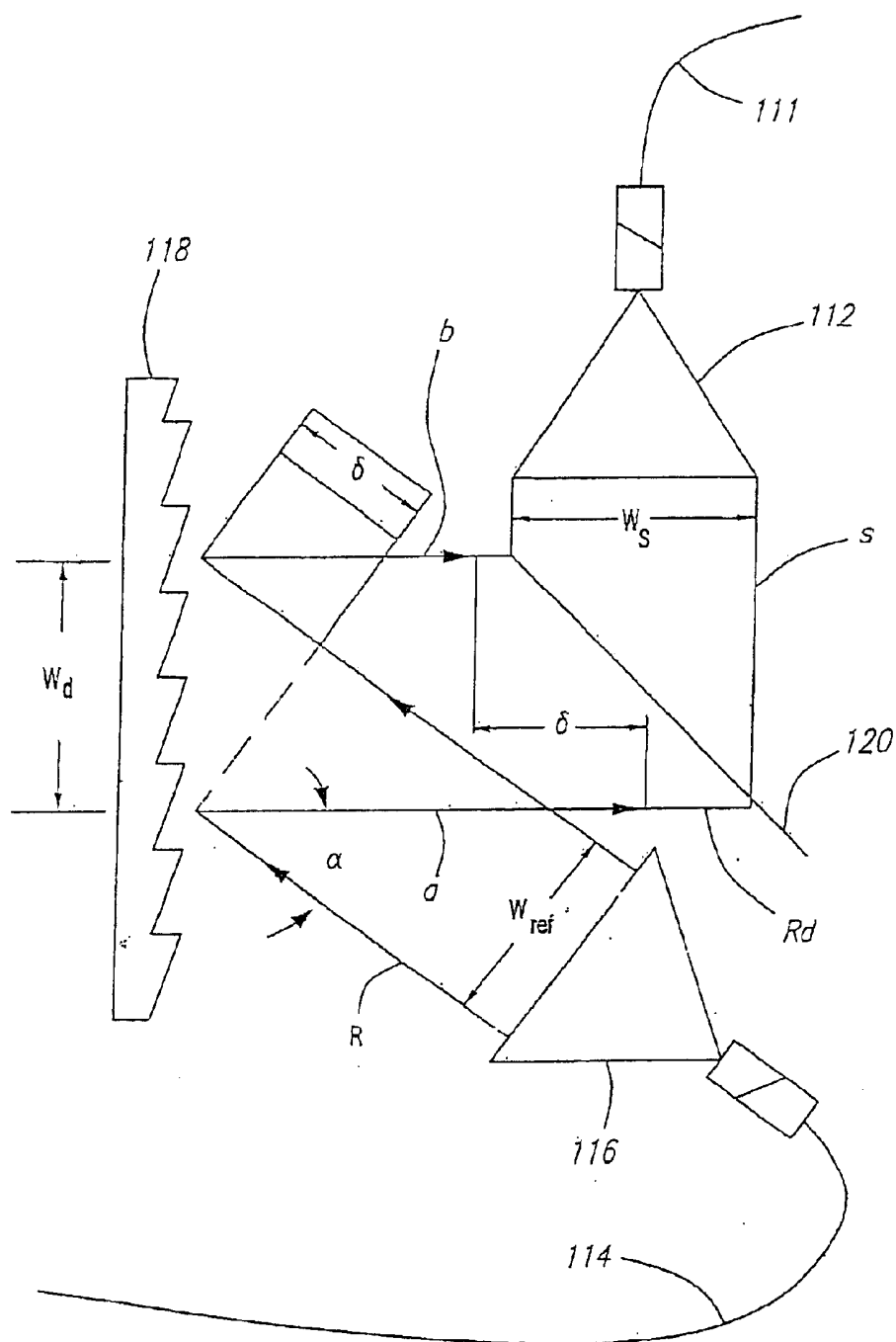


FIG. 10

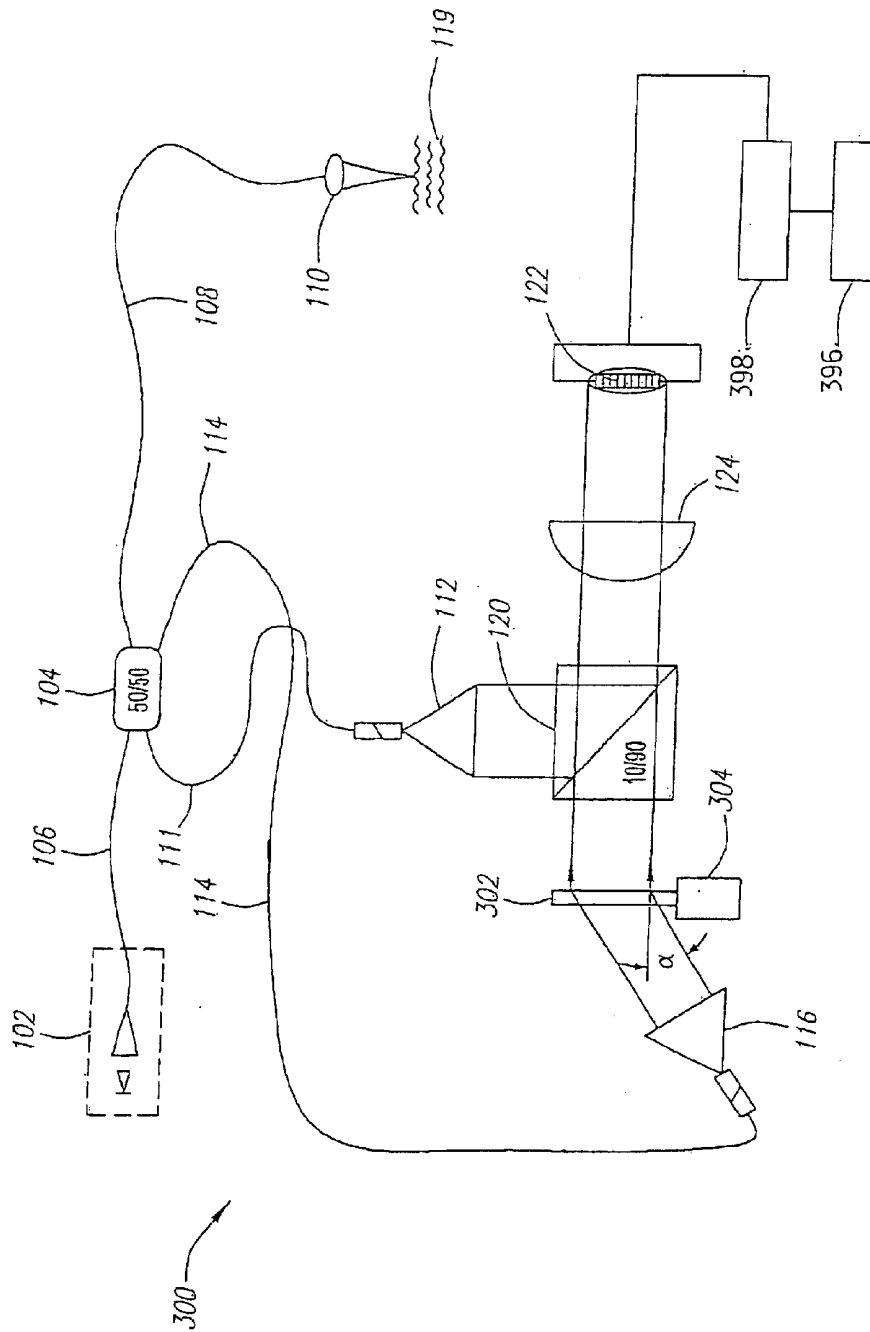


FIG. 11

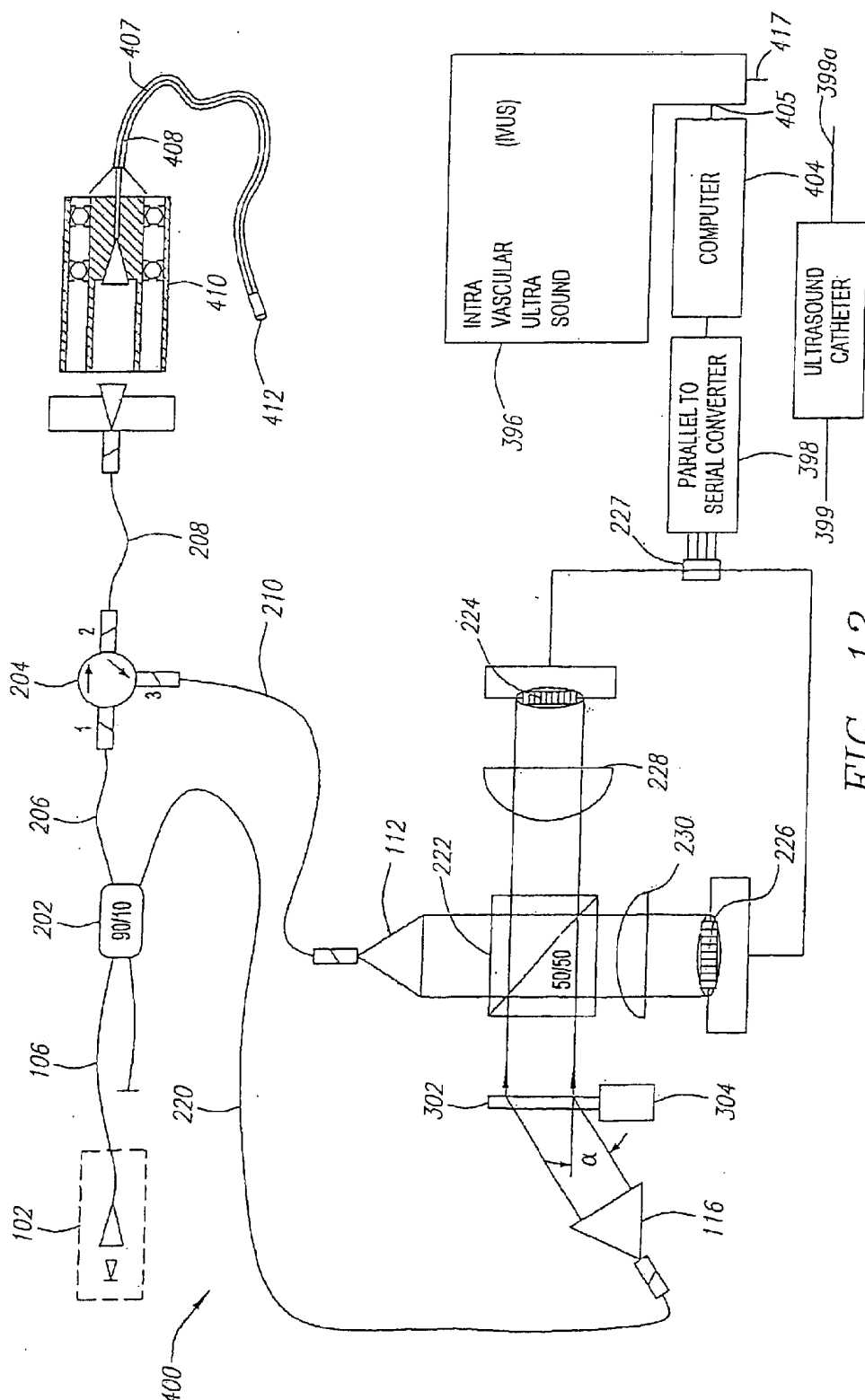


FIG. 12

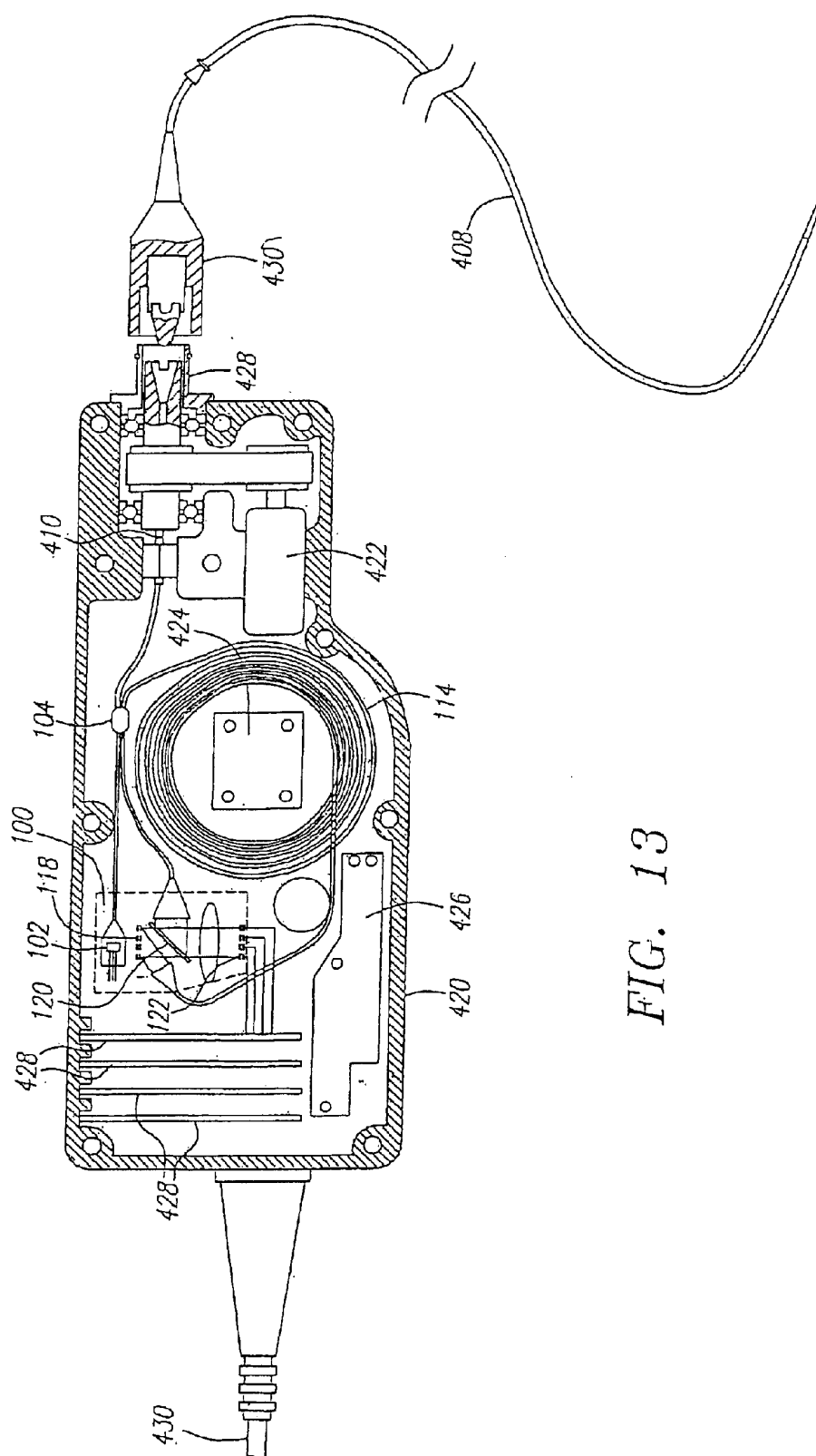


FIG. 13

SYSTEMS AND METHODS FOR PROCESSING SIGNALS FROM AN INTERFEROMETER BY AN ULTRASOUND CONSOLE

RELATED APPLICATIONS

The present application is a continuation-in-part of U.S. patent application Ser. No. 09/909,357, filed on Jul. 18, 2001, and U.S. patent application Ser. No. 09/906,903, filed on Jul. 16, 2001, now U.S. Pat. No. 6,728,571, which are assigned to the assignee of the present application and are incorporated by reference herein, in their entireties. This application is related to U.S. patent application Ser. No. 10/017,534, titled DIFFRACTION GRATING BASED INTERFEROMETRIC SYSTEMS AND METHODS (Attorney Docket No. 265/222), filed on the same day as the present application, assigned to the assignee of the present application and incorporated by reference, herein, in its entirety.

FIELD OF THE INVENTION

The invention relates generally to imaging systems and methods, and, more particularly, to the processing of data from Optical Coherence Tomographic systems.

BACKGROUND OF THE INVENTION

Ultrasound medical imaging is a commonly used procedure to produce images of internal body cavities such as blood vessels and surrounding tissue. In ultrasound imaging of a blood vessel, an Intravascular Ultrasound ("IVUS") catheter is typically inserted into the blood vessel in a known manner. The IVUS catheter comprises an elongated member with an ultrasound transducer located at a distal end of the elongated member. The elongated member is inserted into the blood vessel, and the ultrasound transducer is positioned at a desired location in the blood vessel. The transducer emits ultrasound waves in the blood vessel or other such cavity when excited by a pulse. A portion of the emitted ultrasound waves is reflected back to the ultrasound transducer by tissue boundaries. The reflected ultrasound waves induce an echo signal at the ultrasound transducer. The echo signal is transmitted from the ultrasound transducer to an ultrasound console, which typically includes an ultrasound image processor, such as a computer, and a display. The display may comprise a monitor and/or a printer. The ultrasound console uses the received echo signal to image the cavity.

The echo signal is a serial amplitude modulated signal in which the amplitude of the signal varies with time. A typical echo signal has a time length of 8 μ s, which corresponds to an image depth of approximately 6 millimeters from the ultrasound transducer. The echo signal carries both image brightness information and image depth information, where depth may be taken with respect to the ultrasound transducer. The image brightness information is provided by the amplitude of the echo signal. The image depth information is provided by the time position within the echo signal. An earlier time position in the echo signal corresponds to a lower image depth than a later time position in the echo signal.

In order to produce a radial cross-sectional image of a blood vessel and surrounding tissue, the ultrasound transducer is typically rotated along the axis of the elongated member. As the ultrasound transducer is rotated, the ultrasound transducer emits ultrasound waves in different radial

directions. The resulting echo signals from the different radial directions are processed by the ultrasound console to produce a radial cross-sectional image of the blood vessel and the surrounding tissue. Alternatively, the ultrasonic transducer may be mounted in an assembly together with a reflective member (mirror), where the transducer emits ultrasonic energy in a substantially axial direction and the mirror is oriented to deflect the emitted ultrasonic energy in a radial direction.

Optical Coherence Tomography ("OCT") is a type of optical coherence-domain reflectometry that uses low coherence interferometry to perform high resolution ranging and cross-sectional imaging. In OCT systems, a light beam from a low coherence light source is split into a reference light beam and a sample light beam. A diffraction grating may be used to provide a time delay. The sample light beam is directed onto a sample and the light scattered from the sample is combined with the reference light beam. The combination of the sample and reference light beams results in an interference pattern corresponding to the variation in the sample reflection with the depth of the sample, along the sample beam. The sample beam typically suffers a high loss of energy due to its interaction with the sample. The reference beam serves as a local oscillator to amplify the interference pattern to a detectable level and therefore must have a much higher energy level than the sample light beam. The interference pattern is detected by a photo detector, whose output is processed to generate a cross-sectional image of the sample. High resolution (less than 10 micrometer) imaging of the cross-sections of the sample by OCT is useful in biological and medical examinations and procedures, as well as in materials and manufacturing applications. An advantage of the above-described OCT system is that the array of photo detectors is able to capture image brightness information at multiple image depths in one instance. This enables the OCT system to produce images at true video rates, e.g., 30 frames per second.

OCT based systems may be implemented with fiber optics and an optical fiber carrying the sample light beam may be incorporated into a catheter or an endoscope for insertion into internal body cavities and organs, such as blood vessels, the gastrointestinal tract, the gynecological tract and the bladder, to generate images of internal cross-sections of the cavities or organs. The sample beam is typically emitted from the distal end of the instrument, where a prism or a mirror, for example, directs the sample light beam towards a wall of the cavity. The optical fiber and the prism or mirror may be rotated by a motor to facilitate examination of the circumference of the cavity.

An example of a fiber optic OCT system is shown in U.S. Pat. No. 5,943,133 ("the 133 patent"), where sample and reference light beams are carried in respective optical fibers to a diffraction grating, which introduces a time delay and also combines the sample and reference light beams. FIG. 1 is a schematic diagram of a system 10 disclosed in the '133 patent. The system includes a light source 12 optically coupled to a 50/50 beam splitter 14 through an optical fiber 16. The beam splitter 14 splits the incident light beam equally into a sample light beam and a reference light beam. The sample light beam is carried by an optical fiber 18 to a focusing lens 20, which focuses the sample light beam onto a sample 22. The optical fiber 18 may be contained within a catheter (not shown) for insertion into a body cavity, such as a blood vessel, for examination of the tissue of the wall of the cavity. Light received from the tissue is focused by the lens 20 and coupled back into the optical fiber. The received light travels back to the beam splitter 14, where it is split

again. A portion of the received light is directed into another optical fiber **24**, which conveys the light to a first collimator **26**. The reference light beam travels through an optical fiber **28** to a second collimator **30**. The first and second collimators **26, 30** direct the sample and reference light beams onto the same region of a diffraction grating **32**. The diffracted, combined light beam is conjugated on the detector plane of a multi channel linear diode array detector **34** by a conjugating **36** lens. A neutral density filter (not shown) is provided to decrease the energy in the reference beam to prevent saturation of the detector.

The sample light beam suffers a significant loss of energy due to its interaction with the sample. The second pass through the 50/50 beam splitter further reduces the already attenuated light beam. In addition, the interaction of the light beams with the diffraction grating causes a further loss in both the sample light beam and the reference light beam of about 50% of the incident light in the first order. The diffraction grating also introduces noise. As a result, the system of the '133 patent has a low signal-to-noise ratio.

Another interferometric system using a diffraction grating is described in "Nonmechanical grating-generated scanning coherence microscopy", Optics Letters, Vol. 23, No. 23, Dec. 1, 1998. FIG. 2 is a schematic diagram of the disclosed system **50**. A light source **52** provides light to a 50/50 beam splitter **54** that splits the energy in the light beam equally into a sample light beam **55** and a reference light beam **56**. The sample light beam **55** is directed to a focusing lens **58** that focuses the sample light beam onto a sample **60**. The light received by the focusing lens **58** from the sample **60** is returned to the beam splitter **54**. The reference light beam **56** is directed to a diffraction grating **62** in a Littrow configuration. The diffracted reference light beam is also returned to the beam splitter **54**. The sample and reference light beams are then combined in the beam splitter **54** and directed to a charge-coupled device (CCD) array **64** for detection and processing by a computer **66**. The reference light beam needs to be suppressed here, as well.

Here, only the reference light beam is diffracted, making the system **50** more efficient than the system **10** of the '133 patent, shown in FIG. 1. However, the sample and reference arms in the system **50** of FIG. 2 cannot both be implemented with fiber optics. The diffraction grating introduces a time delay that is spatially spread across the width of the beam. The detector is a multi-element detector at least as wide as the light beam. Each element of the detector receives a portion of the beam corresponding to its position on the diffraction grating. If the reference light beam is conveyed by an optical fiber from the diffraction grating to the detector, the spatial order is lost. If the sample arm is implemented in fiber optics but the reference arm is not, the length of the reference arm would be inconveniently long.

It would be desirable to provide an imaging system that can process both ultrasound imaging data and optical interferometric imaging data with the same signal processor to display both ultrasound images and OADR images, thereby reducing costs.

SUMMARY OF THE INVENTION

In accordance with the present invention, an imaging system is disclosed comprising an ultrasound console having an input and an interferometer comprising a detector with an output coupled to the input of the ultrasound processor to provide data to the ultrasound console. The ultrasound console processes data to form an image for display. The input of the ultrasound console and the output

of the detector are adapted to be selectively coupled. The system may further comprise an ultrasound device with an output that is also adapted to be selectively coupled to the same or another input of the ultrasound console. In that way, either the interferometer or the ultrasound device can be connected to the ultrasound console for use, depending on the particular examination required. The interferometer and the ultrasound device may comprise a catheter.

The detector of the interferometer may be a multi-element detector having a plurality of parallel outputs. A parallel to serial converter may be electrically coupled between the output of the detector and the input of the ultrasound console, to convert the parallel signals outputs by the detector into a serial signal for analysis by the ultrasound console.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a schematic diagram of a prior art OCT system;

FIG. 2 is a schematic diagram of another prior art OCT system;

FIG. 3 is a schematic diagram of an interferometric system connected to an ultrasound console in accordance with one embodiment of the invention;

FIG. 4a is a schematic diagram of a diffraction grating based fiber optic interferometric system in accordance with another embodiment;

FIG. 4b is a schematic diagram of a diffraction grating based interferometric system with a similar arrangement to the system of FIG. 4a, where both beam splitters are 50/50 beam splitters;

FIG. 5 is a schematic diagram of an interferometric system with a similar arrangement to the system of FIG. 4a, where the diffraction grating is a transparent diffraction grating;

FIG. 6 is a schematic diagram of another embodiment of the invention, including an optical circulator and a first, non 50/50 beam splitter;

FIG. 7 is a schematic diagram of the system of FIG. 6, including polarization filters for use in detecting polarization related information;

FIG. 8 is a schematic diagram of the system of FIG. 6, including multiple light sources;

FIG. 9 is a schematic diagram of the system of FIG. 6, including an optical circulator and two non 50/50 beam splitters;

FIG. 10 is an enlarged view of the reference light beam being diffracted by the diffraction grating, indicating the time delay;

FIG. 11 is a schematic diagram of an interferometric system in accordance with another embodiment, wherein an acousto-optic modulator ("AOM") acts as both a transparent diffraction grating to introduce a time delay and as a modulator;

FIG. 12 is a schematic diagram of an AOM based interferometric system, as in the embodiment of FIG. 11, coupled to an ultrasound console; and

FIG. 13 shows an interferometric system in accordance with the embodiment of FIG. 4a, contained within a housing for use with a interferometric catheter and an ultrasound console.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

FIG. 3 is a schematic diagram of an embodiment of an imaging system **390** comprising an interferometric system

391 including a photo detector array 392 with a plurality of parallel outputs 394 connected to an ultrasound console 396 through a parallel to serial converter 398. The ultrasound console may be an intravascular ultrasound ("IVUS") console, including a signal processor, such as a computer, a microprocessor or a microcontroller, and a display to display generated images, as is known in the art. An ultrasound device 399 with an output 399a may also be provided. The output 399a of the ultrasound device 399 may also be connected to the ultrasound console, in the same or a different input than the interferometer 391. A doctor or technician may thereby use either the interferometer 391 for optical imaging or the ultrasound device 399 for ultrasound imaging, with the same ultrasound console. An ultrasound system including an ultrasound image processor and display is available from Boston Scientific Corporation, Natick, Mass. The ultrasound device 399 may be an IVUS catheter. IVUS catheters are described in U.S. Pat. No. 5,715,825 entitled Acoustic Imaging Catheter and the Like, which is incorporated by reference herein, in its entirety. Interferometric systems 391 are described in more detail below.

The parallel to serial converter 398 may be one of the electronic interfaces described in U.S. patent application Ser. No. 09/909,357 ("the '357 application"), entitled "Electronics Interface for an Ultrasound Console", filed on Jul. 18, 2001, assigned to the assignee of the invention and incorporated by reference herein.

As described in the '357 application, the ultrasound console 402 may be configured to receive either an analog or a digital input. In one example of an electronics interface disclosed in the '357 application for receiving an analog input, the electronics interface comprises a plurality of channel processors, each coupled to one of the parallel channel outputs of the photo array. Each channel processor comprises an analog processor, an A/D converter, a First-In-First-Out ("FIFO") memory buffer, and a data bus coupled to the FIFO memory buffer of each one of the channel processors. A single FIFO memory buffer is coupled to the data bus and a D/A converter is coupled to the output of the single FIFO memory buffer. The output of the D/A converter is coupled to the input of the ultrasound console. A controller coupled to an ultrasound motor encoder synchronizes the operation of the electronics interface with the ultrasound console. The operation of the interface is described in more detail in the '357 application.

Where the ultrasound console is adapted to receive a digital input, the serial digital data sequence from the single FIFO memory is provided to the input of the console through control logic that controls the transfer of the digital data sequence, as is also described in the '357 application.

The photo detector array may be a multiplexed photo detector array. Electrical interfaces for single and double channel multiplexed photo detector arrays are also described in the '357 application.

Other electronic interfaces for converting the parallel output of the array of photo detectors into a serial analog or digital data stream, may also be used.

In OCT systems using an array of photo detectors, the array captures image brightness information at multiple image depths in one instance. Since the detected spatial information may be read and stored, the parallel channel outputs of the photo detector array of the interferometric system may be processed into a serial analog or serial digital signal by a parallel to serial converter. The resulting serial signal carries image brightness information and image depth information in a similar manner as a typical echo signal. The

time length and/or frequency of the serial signal may be adjusted to better match the time length and/or frequency of a typical echo signal that the ultrasound console is configured to receive by synchronizing the signal to the sweep speed of the ultrasound scanner and to the propagation velocity of sound. This enables an ultrasound console to process the serial analog signal into an image, in the same way ultrasound data is processed. The same ultrasound console may thereby be used to process both ultrasound based images derived from data received from an ultrasound catheter and optical interferometric based images derived from data received from an interferometric catheter, thereby reducing costs.

The interferometric system 391 may be any OCT interferometric system. For example, the systems of U.S. Pat. No. 5,943,133, and "Nonmechanical grating-generated scanning coherence microscopy", Optics Letters, Vol. 23, No. 23, Dec. 1, 1998, discussed above and incorporated by reference herein, in their entirety, may also be used. Additional interferometric systems are described below.

FIG. 4a is a schematic diagram of one embodiment of a diffraction grating based fiber optic interferometric system 100 that may be used in the imaging system 390 of FIG. 3, shown connected to the IVUS console 396 through the parallel to serial converter 398. The system 100 comprises a light source 102 optically coupled to a fiber optic beam splitter 104 by an optical fiber 106. The fiber optic beam splitter 104 is preferably approximately a 50/50 beam splitter. More preferably, the beam splitter 104 is a 50/50 beam splitter. An optical fiber 108 is optically coupled to the fiber optic beam splitter and to a focusing lens 110.

An optical fiber 111 is also optically coupled to the fiber optic beam splitter 104 such that light entering the beam splitter from the optical fiber 108 is coupled into the optical fiber 110. The optical fiber 111 is also optically coupled to a first collimator 112. Another optical fiber 114 is optically coupled to the first beam splitter 104 and to a second collimator 116.

The optical fibers 108 and 110 comprise first and second parts of a sample arm, respectively, of the interferometric system 100. The optical fiber 114 comprises a reference arm of the system 100. Light from the light source 102 passes through the fiber optic beam splitter 104 and is split into a sample light beam and a reference light beam, each having half of the energy of the initial light beam provided from the light source 102 to the fiber optic beam splitter 104. The sample light beam is directed into the optical fiber 108 of the first part of the sample arm and the reference light beam is directed into the optical fiber 114 of the reference arm. The sample light beam is focused by the focusing lens 110 onto a sample of interest 119, which may be tissue within a body cavity, for example. Light scattered by the sample is focused by the focusing lens 110 to form a second sample light beam and is coupled back into the optical fiber 108 of the sample arm. That light passes back through the first beam splitter 104, where the light beam is split again. A light beam having half of the energy of the received light beam is coupled into the optical fiber 110 of the second part of the sample arm.

The second collimator 116 collimates the reference light beam and directs the reference light beam onto a diffraction grating 118 at an angle α . The diffraction grating 118 introduces an optical path difference to the reference light beam and reflects the diffracted reference light beam onto a second, open space beam splitter 120. The first collimator 112 also collimates the second sample light beam and directs it onto the second beam splitter 120.

The second beam splitter **120** combines the second sample light beam and the reference light beam and directs a portion of the combined light beam onto a photo detector **122**, through a conjugating lens **124**. The photo detector **112** is preferably a multi-element photo detector, such as a photo diode array. An array of avalanche mode photo diodes may be used, for example. A charge coupled-device ("CCD") may be used, as well. The conjugating lens **124** projects the image of the combined beam on the plane of the second beam splitter onto the detector plane.

In accordance with this first embodiment, the open space beam splitter **120** directs less than half of the light energy in the reference beam and more than half of the energy in the second sample light beam into the combined beam directed toward the detector **122**. Preferably, substantially more than half of the energy in the second sample light beam, such as 75% or more, is directed into the combined beam and substantially less than half of the energy in the reference light beam, such as 25% or less, is directed into the combined light beam. More preferably, at least about 90% or more of the energy of the sample light beam and about 10% or less of the energy of the reference light beam are directed into the combined beam. For example, the second beam splitter may be a 10/90, 5/95, 2/98 or 1/99 beam splitter. In the embodiment of FIG. 3, the reference light beam is transmitted through the second beam splitter **120** while the sample light beam is reflected by the second beam splitter **120**. Alternatively, the sample light beam may be transmitted through the second beam splitter **120** and the reference light beam may be reflected by the second beam splitter.

As is known in the art, in order for there to be constructive interference between the sample and reference light beams in this and the other embodiments of the invention, the optical path lengths of the sample light beam (the initial sample light beam and the second light beam) and the reference light beam from the first beam splitter **104** to the second beam splitter **120** need to be equal to within the coherence length of the light source **102**. The refractive index of the optical fibers and the open space traversed by the light beams, as well as the refractive index of the sample material, need to be considered in determining appropriate path lengths.

The interference pattern resulting from the combination of the sample and reference light beams contains both depth information and brightness information. The brightness information is provided by the light intensities of the interference pattern. Since the portion of the second sample light beam that is received in the sample arm from a certain depth from the sample interferes with a portion of the diffracted reference beam at a spatial position corresponding to the optical path difference for this position, the depth information is provided by the spatial position within the interference pattern. The photo detectors of the array **122** are arranged so that each photo detector element detects the light intensity of the interference pattern at a certain spatial position within the interference pattern, as is known in the art. Thus, the output of each photo detector element provides image brightness information for a certain image depth. The array **122** outputs the information along parallel channels (not shown), where each channel corresponds to the output of one of the photo detector elements. The outputs of the parallel channels of the photo array **122** are provided to the IVUS console **396** through the parallel to serial converter **398** to produce an image of the sample depth reflection along the sample light beam for display. Preferably, the multi-element detector **122** is a photo diode array and a heterodyne detection technique is used.

As discussed above, if the detector is a photo diode array and a heterodyne detection method is used, low frequency modulation is required. A modulator **117**, such as a fiber stretcher or an acousto-optic modulator, is therefore provided along the optical fiber **114**. The modulator **117** may be provided along the optical fibers **108** or **111** to modulate the sample light beam, as well.

Use of two beam splitters enables the reference light beam to be conveyed to the diffraction grating **118** by an optical fiber **114**. Since the second sample light beam is not combined with the reference light beam on the diffraction grating in this embodiment, additional loss and noise is not introduced to the second sample light beam. Since the optical path from the diffraction grating **118** to the detector **122** is open space, spatial information in the reference and sample light beams is preserved.

The optical fiber **108** of the first part of the sample arm is preferably incorporated in a catheter adapted to be positioned in a body cavity or organ by standard catheter intervention procedures. For example, the catheter may be inserted into a blood vessel or the heart by guiding the flexible catheter through various blood vessels along a circuitous path, starting, for example, by percutaneous introduction through an introducer sheath disposed in a perforation of the femoral artery. Alternatively, the catheter can be introduced directly into a body cavity or body tissue, such as an organ. The optical fiber may be coupled to a motor for causing rotation of the fiber within the catheter. Catheters and endoscopes for use in the optical imaging of blood vessels and other internal body cavities are known in the art and are described in U.S. Pat. No. 6,134,003, U.S. Pat. No. 5,321,501 and International Publication No. WO 98/38907 published on Sep. 11, 1998, for example, which are incorporated by reference herein. As disclosed in those references, a mirror or prism may be provided to reflect the sample light beam onto biological tissue parallel to the optical fiber and to reflect light received from the tissue into the optical fiber. By rotating the optical fiber, tissue along the circumference of the cavity may be examined.

While it is preferred that the second beam splitter **120** in FIG. 4a be a non 50/50 beam splitter, it is not required. FIG. 4b is a schematic diagram of an interferometric system **100'** that is similar to the system of FIG. 4a, except that the second beam splitter **120'** is a 50/50 beam splitter. A neutral density filter or other such attenuator may be provided as needed to suppress the reference light beam to prevent saturation of the detector **124**. Components common to the embodiment of FIG. 4a are commonly numbered.

FIG. 5 is a schematic diagram of another interferometric system **150** that may be used in the imaging system **390**. The interferometric system **150** has a similar arrangement to the system **100** of FIG. 4a, except that the diffraction grating is a transparent diffraction grating **152**. Components common to the configuration of FIG. 4a are commonly numbered in FIG. 5. The second collimator **116** is arranged to direct the reference light beam on a rear side of the diffraction grating **152** at an angle α . The diffracted reference beam is directed onto the open space beam splitter **120**, for combination with the second sample light beam, as discussed above. The combined light beam is directed through the conjugating lens **124** and onto the multi-element detector **122**, also as described above. The ability to use either a reflective diffraction grating **118** or a transparent diffraction grating **152** in the interferometric systems of the invention, adds flexibility to the design of the interferometer in practical applications. Any of the embodiments described herein can use either a reflective or a transparent diffraction grating.

FIG. 6 is a schematic diagram of another embodiment of an interferometric system **200** that can be used in the imaging system **390**, wherein more than half of the light energy is directed into the sample light beam and less than half of the light energy is directed into the reference light beam by use of a non 50/50 fiber optic beam splitter. Preferably, substantially more than half of the light energy incident on the beam splitter, such as 75% of the energy, is directed into the sample light beam and substantially less than half of the incident light energy, such as 25%, is directed into the reference light beam. More preferably, at least about 90% of the incident light energy is directed into the sample light beam and about 10% or less is directed into the reference light beam.

In this embodiment, the sample light beam is directed to and from the sample under examination through an optical circulator instead of a beam splitter, as in the embodiment of FIG. 4a and in the prior art of FIGS. 1 and 2. Therefore, the first beam splitter need not be approximately a 50/50 beam splitter.

Components common to the embodiment of FIG. 4a are commonly numbered in FIG. 6. A light source **102** provides light to a 90/10 beam splitter **202** through an optical fiber **106**. The 90/10 fiber optic beam splitter **202** provides 90% of the energy of the light incident to the beam splitter **202** into the sample light beam and 10% of the energy of the light into the reference light beam.

An optical circulator **204** is provided with three ports, Port 1, Port 2 and Port 3. Light entering the optical circulator **204** through Port 1 is directed out of the circulator through port 2. Light entering the optical circulator **204** through Port 2 is directed out of the circulator through Port 3. An optical fiber **206** is optically coupled to the first beam splitter **202** to Port 1 of the optical circulator **204** to convey the sample light beam to the circulator.

An optical fiber **208** is optically coupled to Port 2 of the optical circulator **204** and to a focusing lens **110**. An optical fiber **210** is optically coupled to Port 3 of the optical circulator **204** and to a first collimator **112**. The sample light beam is conveyed from the first beam splitter **202** to Port 1 of the optical circulator **204** through the optical fiber **206**. The sample light beam is directed to Port 2 of the optical circulator, where it exits the circulator and is conveyed to the focusing lens **110** by the optical fiber **208**. The focusing lens focuses the sample light beam onto the sample **119**. Light received from the sample is focused and coupled into the optical fiber **108**, forming a second sample light beam to be returned to Port 2 of the optical circulator. The second sample light beam is directed from Port 2 to Port 3 of the optical circulator, where it is conveyed by the optical fiber **204** to the first collimator **112**.

An optical fiber **220** is also optically coupled to the beam splitter **202** and to a second collimator **116**, as in the embodiment of FIG. 4a. A reference light beam having 10% of the energy of the light conveyed to the 90/10 beam splitter **202** from the light source **102** is directed into the optical fiber **220**. The second collimator **116** directs the reference light beam onto a reflective diffraction grating **118**. The diffraction grating **118** introduces an optical path difference to the reference light beam and reflects the diffracted reference light beam onto the open space beam splitter **120**. A transparent diffraction grating **152** could be used instead of the reflective diffraction grating **118**, as discussed above. The first collimator **112** also directs the second sample light beam onto the open space beam splitter **120** for combination with the reference light beam.

In this embodiment, the second beam splitter **120** is approximately a 50/50 beam splitter **222**. Preferably, the second beam splitter **120** is a 50/50 beam splitter. Two combined sample/reference beams, each having half of the energy of the second sample light beam and half of the energy of the reference light beam, are formed. Two photo detectors **224**, **226**, which are preferably multi-element photo detectors, are provided, one along the path of each combined light beam. Because two detectors are provided, the 50/50 beam splitter **222** does not cause a loss of energy and information in the second sample light beam. Respective conjugating lenses **228**, **230** are provided between each detector **224**, **226** and the second beam splitter **222**. The outputs of individual detectors in corresponding spatial positions in each array are combined by analog circuitry **227**. The parallel output of the analog circuitry **227** is provided to the IVUS console **396** through the parallel to serial converter **398**, for processing into an image in a manner known in the art. Two detectors may be readily provided in the embodiment of FIG. 4b, as well, in the same manner.

Preferably, about 90% or more of the light energy is directed into the sample light beam and about 10% or less of the light energy is directed into the reference light beam by the first beam splitter **202**. The amount of energy provided to the sample and reference beams may be controlled by selection of the characteristics of the fiber optic beam splitter **202** so that only the necessary amount of light energy is provided to the reference light beam to sufficiently amplify the sample light beam for imaging without saturating the multi-element photo detectors **224**, **226**. The remainder of the energy is directed to the sample light beam. A 2/98, a 95/5 or a 1/99 or other such beam splitter may also be used, for example.

Directing the second sample light beam received from the sample **119** through the optical **204** circulator **204** instead of back through the first beam splitter **202** avoids a significant source of loss in the second sample beam. The loss in the optical circulator is between about 0.5 decibels ("db") to about 1.1 db each way. The two way loss in the optical circulator is therefore about 1.0 db to about 2.2 db (about 37%). The loss in a 50/50 beam splitter **222**, by contrast, is 50% each way or 75% if the sample beam travels through the 50/50 beam splitter twice.

The detectors **224**, **226** may be tuned to detect light at the same wavelength band or at different wavelength bands. The ability to detect more than one wavelength band is useful for spectroscopy and for reducing aliasing in the image.

The two combined sample/reference light beams in the embodiment of FIG. 6 may contain polarization related information. Birefringence measurements may be made by providing a polarization filter along each light beam, where each filter allows passage of light having a different polarization. In FIG. 7, polarizations filters **240**, **242** are shown between each of the conjugating lenses **228**, **230** and the detectors **224**, **226**, respectively. The detectors are preferably multi-element photo detectors. Two parallel to serial converters **398a**, **398b** may be provided, one to receive the parallel outputs from each multi-element detector. The outputs from the parallel to serial converters **398a**, **398b** may be provided in parallel to the IVUS console **396**. Two images may be generated and compared. Differential measurements may be made by comparing the signals at each detector as a function of spatial position and relative intensity, as is also known in the art. Variations in intensity versus position are an indication of polarity sensitive areas of target tissue. The optical fiber used in this embodiment is preferably a polar-

ization maintaining (high birefringence) optical fiber, as is known in the art. A polarization filter **243**, shown in phantom, may also be provided between the light source **102** and the fiber optic beam splitter **202** instead of the polarization filters **240**, **242**, to polarize the light beam emitted by the light source to a desired polarization. Instead of the polarization filter **243**, the second beam splitter **222** may be a polarization beam splitter. A single detector, as in the embodiments of FIGS. **3** and **4**, may also be used to detect a light beam of a particular polarization.

Polarization filters may be provided in other interferometric systems where two combined beams are formed, as well. For example, a 50/50 beam splitter may also be provided between the diffraction grating **32** and the detector **34** in the system of the '133 patent shown in FIG. **1**, to form two combined beams. A second detector, two polarization filters and two conjugating lenses may then be provided, as in FIG. **7**, to conduct birefringence measures.

In another variation in the embodiment of FIG. **6**, a second light source **103** may be provided, as shown in FIG. **8**. Additional light sources may also be provided. Each light source may emit light at a different wavelength. For example, the first light source can emit light at 800 nanometers and the second light source can emit light at 1200 nanometers. The light from the second light source **103** may be coupled into the optical fiber **106** by a wavelength division multiplexor, for example. One of the detectors **224**, **226** may be tuned to detect light at a wavelength corresponding to the first light source **102** and the other detector may be tuned to detect light at a wavelength band corresponding to the second light source **103**. If more than two light sources are provided, the individual photo detectors in each array can be tuned to detect light at different wavelength bands. As in the embodiment of FIG. **7**, two parallel to serial converters **398a**, **398b** may be provided with separate outputs to the IVUS console **396**. Images at each wavelength band may be generated. The interference patterns at each wavelength band may be compared as a function of spatial position and intensity at each wavelength band. The difference in intensity at the same position in the interference patterns may indicate wavelength dependent attenuation or absorption of the sample. Bandpass filtering, detector response and the fiber characteristics of each "detection channel" may be selected to optimize the use of specific wavelengths.

Fluorescence of tissue is known to be dependant upon tissue type and tissue constituents. One of the light sources in FIG. **8** may be in the blue or ultraviolet range, for example, to induce fluorescence in the tissue. One of the detectors **224**, **226** may be tuned to the ultraviolet, blue or other wavelength band at which the target tissue is expected to fluoresce to detect the intensity of the emitted fluorescent light.

In another embodiment using an optical circulator **204**, neither the first fiber optic beam splitter nor the second open space beam splitter is a 50/50 beam splitter. In the system **280** of FIG. **9**, the first beam splitter **282** is a 95/5 beam splitter, for example, that directs 95% of the light energy provided to the beam splitter into the sample light beam and 10% into the reference light beam. The second open space beam splitter **284** is a 10/90 beam splitter, for example, directing 90% of the light energy in the second sample light beam and 10% or less of the light energy in the reference light beam toward a single detector **286** in the combined beam. Varying the characteristics of both beam splitters **282**, **284** provides additional flexibility in optimizing the energy distribution between the sample and reference light beams. Components of the system **280** common to the embodiments of FIGS. **6** and **4a** are commonly numbered.

To determine the theoretical percentage of the light source energy reaching the detector from the sample arm in the

various embodiments of the invention and in the prior art, the sample under examination may be replaced by a mirror. The table below shows the percentage of the light source energy in the sample and reference arms at the sample, at the diffraction grating and at the detector in the prior art interferometer of FIG. **1** and in the example interferometers of FIGS. **4a**, **5** and **6**, if the sample light beam is reflected by a mirror (suffers no loss due to interaction with the sample).

Figure	Percentage of light source energy incident on:				
	Sample Arm	Diffraction Grating		Detector/Detectors	
		Sample Arm	Reference Arm	Sample Arm	Reference Arm
FIG. 1	50	25	50	12.5	25
FIG. 4a	50	NA	50	22.5	2.5
FIG. 5	50	NA	50	22.5	2.5
FIG. 6	90	NA	10	56.7	5

In the prior art of FIG. **1**, the light energy in the reference light beam incident on the detector is 25% of the light energy from the source and is higher than the sample light energy. To prevent saturation of the detector, the reference beam has to be suppressed. In the embodiments of FIGS. **4a** and **5**, in the sample arm, the light source energy is reduced by 75% by two passes through the 50/50 beam splitter and then by 10% by the 10/90 beam splitter. In the reference arm, the light source energy is reduced by 50% by the first beam splitter, 50% by the diffraction grating and 90% by the second beam splitter. In the embodiment of FIG. **6**, in the sample arm, the light source energy is reduced by 10% by the 90/10 beam splitter and by 37% by two passes through the optical circulator. The loss caused by the 50/50 beam splitter does not reduce the total energy of the sample light beam because the total energy of the light incident on both detectors by the sample light beam is the same as the energy of the sample light beam incident on the beam splitter. In the reference arm, the light is reduced to 10% of the light energy from the source by the 10/90 beam splitter and then by 50% by the diffraction grating. In the embodiments of FIGS. **4a**, **5** and **6**, the proportion of the initial light energy in the reference light beam incident on the detector is much lower than in the prior art and the proportion of the light energy in the sample light beam is higher. Saturation of the detector or detectors may be readily avoided by suitable selection of the characteristics of the beam splitters. A neutral density filter may be provided along the reference arm for more precise control over the energy of the reference light beam, if necessary. Since more of the light energy from the source may be allocated to the sample light beam, where it is most needed, less energy is wasted in the system.

FIG. **10** is an enlarged view of the reference light beam **R** emitted by the collimator **116** being diffracted by the diffraction grating **118**, showing the maximum optical path difference δ across the diffracted reference light beam **Rd** for the embodiment of FIG. **4a**. The second sample light beam **S** received from the sample is shown being emitted by the collimator **112**. The second beam splitter **120** is also shown. The optical path difference δ varies gradually across the diffracted reference light beam **Rd** such that the difference at one side of the beam cross-section "a" is about zero and the difference at the opposite side of the beam "b" is the maximum difference δ . The maximum optical path difference δ is typically chosen to enable measurement of the light scattered from the desired depth. Since the optical paths of the reference and sample light beams have to be substantially equal, the optical path difference δ corresponds to the depth of the image in the second sample light beam **S**,

corrected by the refractive index of the media in which the depth is measured. The maximum optical path difference δ is a function of the width W_d of the diffracted light beam and the angle of incidence α :

$$\delta = W_d \sin \alpha. \quad (1)$$

The depth Δ is a function of the maximum optical path difference δ . Since it takes a two-way sample beam path to determine the depth versus a one way reference beam path to define the maximum optical path difference, the depth is half of the maximum optical path difference δ . Since the depth Δ is measured in a material other than air, it is also a function of the refraction coefficient of the sample material η :

$$\Delta = \delta / 2\eta. \quad (2)$$

The angle of incidence α of the reference light beam on the diffraction grating is a function of the diffraction grating parameter p (distance between adjacent grooves) and the light wavelength λ . The diffraction grating formula is:

$$\sin \alpha = \lambda / p. \quad (3)$$

Also, as shown in FIG. 10, the width W_{ref} of the reference light beam R is less than the width W_d of the diffracted reference light beam R_d . Preferably, the width W_d of the diffracted reference light beam is the same as the width W_s of the second sample light beam S . The combined light beam (not shown) has the same width. The width W_{ref} of the reference light beam is therefore preferably:

$$W_{ref} = W_s / \cos \alpha \quad (4)$$

The width of the detector array or arrays should be the same or slightly greater than the width of the combined light beam. Preferably, the first collimator 112, that collimates the second sample light beam S received from the sample, has the same dimensions as that of the detection array.

For example, if the sample is biological tissue ($\eta=1.33$) and the depth of measurement is $\Delta=3$ mm, the maximum optical path difference from formula (2) would be: $\delta=7.98$ mm. If the light source has a wavelength $\lambda=820$ nm and the diffraction grating parameter is $p=1/830$ mm, the angle α from formula (3) would be: $\sin \alpha=0.697$ ($\alpha=44.2$ deg.). Then, the width W_d of the diffracted reference beam R_d , which is preferably equal to the width W_s of the second sample light beam received from the sample W_s from (1) would be $W_d=11.45$ mm. The width of the combined light beam is also W_d . The photo detector array would then also have a width of at least 11.45 mm.

In the embodiments above, the light source 102 is a low coherence, broadband light source, such as a super luminescent diode. The coherence length of the light source may be from about 15 to about 30 microns, for example. The wavelength may be between about 800 to about 1500 nanometers, for use with biological tissue. The light source should emit light at a power of at least about 10 milliwatts for depth measurements of about 1 millimeter. The light source should emit light at a power of at least about 50 milliwatts for depth measurements of 2–3 millimeters. Superluminescent diodes for use in the embodiments may be obtained from Super Lume Diodes, Ltd. Moscow, Russia, or Hamamatsu Photonics K. K., Solid State Division, Hamamatsu City, Japan, ("Hamamatsu") for example.

The detector is preferably a multi-element photo detector, such as a photo diode array. An avalanche mode photo diode array may be used, for example. The photodiode array preferably has at least 256 diodes. An array of 512 photo diodes or more is more preferred. Photo diode arrays may be obtained from Sensors Unlimited, Inc., Princeton, N.J. and

Hamamatsu, for example. A charge-coupled device ("CCD") may also be used.

Appropriate optical fibers and fiber optic beam splitters of desired characteristics are readily commercially available. They may be obtained from Corning Incorporated, Corning, N.Y., for example. Open space beam splitters of desired characteristics are also readily commercially available. They may be obtained from Edmunds Scientific, Tonawanda, New York, for example. The conjugating lenses and focussing lens may also be obtained from Edmunds Scientific, for example.

FIG. 11 is yet another embodiment of an interferometric system 300, that may be used in the imaging system 390 of FIG. 3, wherein an acousto-optic modulator ("AOM") 302 acts as both a transparent diffraction grating to introduce an optical path difference to the reference light beam and as a modulator to introduce a frequency shift. Otherwise, the system is the same as the embodiment of FIG. 4a. One AOM may be used for shallow depths of a few hundred microns, for example. Two modulators may be used for greater depths of 500 to 1,000 microns, for example. One AOM may also be used along with a transparent diffraction grating, as shown in U.S. Pat. No. 6,114,645, which is incorporated by reference herein. While one AOM may introduce a frequency of modulation higher than that desirable in an OCT system, two or more AOM's in series, each driven at different frequencies, may be used to achieve the desired frequency. The AOM 302 may be driven by a programmable signal generator, as is known in the art.

Since the projected interference pattern generated by the interferometric system of the invention is formed on the detector nearly instantaneously, pulsed imaging may also be implemented in any of the embodiments discussed above. Pulsed imaging allows for the use of higher peak power and lower average power (lower duty cycle), enabling increased penetration through attenuative structures while maintaining low average light energy for safe operation. A laser diode may be used in a pulsed mode as the light source in any of the embodiments. The laser diode may be smaller and less expensive than the superluminescent diode discussed above for continuous operation, because a small laser diode may produce a sufficient peak output at a wider bandwidth in a pulse mode without being destroyed.

FIG. 12 shows an imaging system 391 including an AOM based interferometric system 400, as in the embodiment of FIG. 11, wherein the first, fiber optic beam splitter 202 is a 90/10 beam splitter and the second, open space beam splitter 222 is a 50/50 beam splitter. Two photo detector arrays 224, 226 are provided, as in the embodiment of FIG. 6. The outputs of corresponding detectors in each of the parallel outputs from the photo detector arrays 224, 226 of the interferometric system 400 are combined by analog circuitry 227, as noted above. The parallel outputs of the analog circuitry 227 are input to the parallel to serial converter 398 that converts the parallel outputs into a serial amplitude modulated signal that can be processed by an ultrasound console. If only one detector is provided, as in the embodiment of FIG. 4a, for example, the analog circuitry 227 is not needed and the parallel outputs of the photo detector array 122 could be provided directly to the parallel to serial converter 398.

A computer 404 may optionally be provided to process the serial signal output by the parallel to serial converter. The serial signal is then provided to the IVUS console 396 through an input 405 for processing into an image for display. The interferometric system 400 may be selectively connected to the input 405 when optical imaging is desired. The ultrasound catheter 399 is also shown in FIG. 12, with an output 399a. The output 399a may be connected to the input 405 or a separate input 417 of the IVUS console 396 when ultrasound imaging is desired.

The optical fiber 208 of the sample arm is shown coupled to an optical fiber 407 within a catheter 408 through a rotary connector 410. A mirror or prism 412 is shown for reflecting the sample light beam out of the catheter to tissue in a body cavity, as described above. The rotary connector 410 is driven by a motor, as is known in the art.

FIG. 13 shows a housing 420 containing an interferometer in accordance with the embodiment of FIG. 4a of the present invention for use with an interferometric catheter 408 and an IVUS console 396. Components common to the other embodiments are commonly numbered. The light source 102, the fiber optic beam splitter 104, the optical fibers 106, 108, 110 and 114, the diffraction grating 118, the collimators 112, 116, the open space beam splitter 120, the conjugating lens 124 and the multi-element detector 122 are shown. The rotary coupler 410 of FIG. 11 is also shown. A motor 422 is provided in the housing 420 to rotate the rotary coupler 410 and the optical fiber 407 within the catheter 408. A motor controller 424 controls the operation of the motor 422. A power supply 426 is shown, as well. Data acquisition and processing boards 428 are provided, electrically connected to a cable 430 for connection to the IVUS console 396. The parallel to serial converter 398 may be included on the processing boards. A port 428 of the housing and a catheter adapter 430 for connection to the port are shown as well.

As mentioned above, any of the embodiments of the interferometric systems described herein, as well as other fiber optic and non fiber optic OCT systems using a multi-element photo detector, may be used in the imaging system 390.

While use of a multi-element photo detector array is preferred, a single element photo detector may also be used, in which case the width of the combined light beam could be moved across the detector or the detector could be moved across the width of the combined light beam.

Another interferometric system which may be used is described in U.S. Ser. No. 09/906,903, entitled "Electronically Scanned Optical Coherence Tomography with Frequency Modulated Signals", filed on Jul. 16, 2001, assigned to the assignee of the present invention and incorporated by reference herein. There, an interferometer uses a single element detector and image depth information is carried on multiple modulation frequencies, each corresponding to a different depth. The image depth information in the signal output by the detector may be resolved by tuning to the desired frequency. Interfaces for coupling interferometer with a single element detector to an IVUS console are also disclosed.

Alternatively, an oscillating mirror or other such reflector may be used to scan a sample depth. For example, interferometers such as those described in U.S. Pat. No. 6,134,003, U.S. Pat. No. 6,111,645, U.S. Pat. No. 5,459,570, U.S. Pat. No. 5,321,501 and International Publication No. WO 98/38907 published on Sep. 11, 1998, for example, which are also incorporated by reference herein, may also be used in the imaging system with an interface disclosed in the '903 application or other such interfaces.

As was also mentioned above, the sample arm may be incorporated in an endoscope for insertion into the gastrointestinal tract, for example. The sample arm may also have a probe at its end for examining external biological tissue, such as the eye, or other types of samples, such as semiconductors.

While the preferred embodiments described above are implemented with fiber optics for use in examining internal biological tissue, such as biological tissue along internal body cavities and organs, the embodiments of the invention may be readily implemented with bulk optics or other optical components. In a non fiber optic implementation, one collimator is preferably provided between the light source and the first beam splitter.

While use of a multi-element photo detector array is preferred, a single element photo detector may also be used, in which case the width of the combined light beam could be moved across the detector or the detector could be moved across the width of the combined light beam.

Use of a focusing lens, first and second collimators and one or two conjugating lenses are also preferred, but not required.

While various embodiments of the invention have been described, it will be apparent to those of ordinary skill in the art that modifications may be made to those embodiments without going beyond the spirit and scope of the invention, as defined by the following claims and their equivalents.

We claim:

1. An imaging system comprising:

an ultrasound console having a serial input;

an interferometer comprising a multi-element photo detector, having a plurality of parallel outputs, wherein the multi-element photo detector is configured to detect the light intensity of an interference pattern, and

a parallel to serial converter electrically coupling the plurality of parallel outputs of the multi-element photo detector to the serial input of the ultrasound console, wherein the ultrasound console processes data provided by the interferometer to form an image for display.

2. The imaging system of claim 1, wherein the ultrasound console further comprises a second input and the system further comprises an ultrasound device with an output coupled to the second input.

3. The imaging system of claim 1, wherein the interferometer comprises a catheter.

4. The imaging system of claim 2, wherein the ultrasound device comprises a catheter.

5. The imaging system of claim 1, wherein the ultrasound console is configured to process analog serial data and the parallel to serial converter is adapted to provide analog serial data to the ultrasound console.

6. The imaging system of claim 1, wherein the ultrasound console is configured to process analog serial data and the parallel to serial converter is adapted to provide digital serial data to the ultrasound console.

7. The imaging system of claim 1, wherein the interferometer comprises two multi-element photo detectors, each comprising a plurality of parallel outputs coupled to the parallel to serial converter.

8. The imaging system of claim 1, wherein the interferometer further comprises:

a light source;

means for creating a sample light beam and a reference light beam from light from the light source;

means for conveying the sample light beam to a sample;

means for introducing a time delay into at least one of a second sample light beam received from the sample and the reference light beam; and

means for combining the second sample light beam with the reference light beam to form a combined light beam for detection by the detector.

9. The imaging system of claim 8, wherein the means for combining the second sample light beam and the reference light beam is a beam splitter.

10. The imaging system of claim 8, wherein the means for introducing a time delay and the means for combining the second sample light beam and the reference light beam is a diffraction grating.

11. The imaging system of claim 8, wherein:

the means for introducing a time delay is a diffraction grating that introduces the time delay to the reference light beam; and

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the means for combining the second sample light beam and the reference light beam is a beam splitter.

12. The imaging system of claim 8, wherein the means for forming the sample and reference light beams is a first beam splitter and the means for combining the second sample light beam and the reference light beam is a second beam splitter.

13. The imaging system of claim 1, wherein the interferometer further comprises:

a low coherence light source;

a first beam splitter in communication with the light source to split light from the light source into a sample light beam to be directed onto a sample and a reference light beam;

a diffraction grating in communication with the first beam splitter to receive the reference light beam from the first beam splitter and to diffract the reference light beam; and

a second beam splitter positioned to receive a reflected sample light beam from the sample, the second beam splitter being in communication with the diffraction grating to receive the diffracted reference light beam, wherein the reflected sample light beam and the diffracted reference light beam are combined in the second beam splitter to form a combined light beam; and a detector positioned to receive the combined light beam from the second beam splitter.

14. The imaging system of claim 13, wherein at least one of the first beam splitter and the second beam splitter is a non 50/50 beam splitter.

15. The imaging system of claim 14, wherein:

the first beam splitter is an approximately 50/50 beam splitter; and

the second beam splitter directs more than half of the light energy in the reflected sample light beam into the combined beam and directs less than half of the light energy in the reference light beam into the combined beam.

16. The imaging system of claim 15, wherein the second beam splitter directs substantially more than half of the light energy in the reflected sample light beam into the combined light beam and directs substantially less than half of the light energy in the reference light beam into the combined beam.

17. The imaging system of claim 16, wherein the diffraction grating is a reflective diffraction grating, a transparent diffraction grating or an acousto optic modulator.

18. The imaging system of claim 14, wherein the first beam splitter directs more than half of the light energy received from the light source into the sample light beam and less than half of the light energy received from the light source into the reference light beam.

19. The imaging system of claim 18, further comprising an optical circulator, wherein the sample light beam is directed to the sample through the optical circulator and the reflected sample light beam is directed to the second beam splitter through the optical circulator.

20. The imaging system of claim 19, wherein the second beam splitter directs substantially more than half of the light energy received from the light source into the sample light beam and substantially less than half of the light energy received from the light source into the reference light beam.

21. The imaging system of claim 20, wherein the second beam splitter is an approximately 50/50 beam splitter and the reflected sample light beam and the reference light beam are combined in the second beam splitter to form first and second combined light beams, the first light beam being detected by the first detector; and

the interferometer further comprises a second detector to detect the second light beam.

22. The imaging system of claim 1, further comprising a focusing lens to focus the sample light beam onto the sample and to focus the reflected sample light beam.

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23. An imaging system comprising:

an ultrasound console having an input;

an interferometer comprising:

a low coherence light source;

a first fiber optic beam splitter;

a first optical path optically coupling the light source to the first beam splitter, wherein the first beam splitter splits light received from the light source into a sample light beam and a reference light beam;

a second optical path optically coupling the first beam splitter to a sample and coupling a reflected sample light beam from the sample to the first beam splitter a second beam splitter;

a third optical path optically coupling the first beam splitter to the second beam splitter to convey the reflected sample light beam, at least in part, from the first beam splitter to the second beam splitter;

a diffraction grating;

a fourth optical path optically coupling the first beam splitter to the diffraction grating to convey the reference light beam, at least in part, to the diffraction grating;

wherein the second beam splitter is positioned to receive the diffracted reference light beam and the reference light beam and the reflected sample light beam are combined in the second beam splitter to form a combined light beam; and

a multi-element photo detector having a plurality of parallel outputs, the multi-element photo detector being positioned to receive the combined light beam;

the system further comprising a parallel to serial converter comprising a plurality of inputs, each input being coupled to a respective one of the plurality of outputs of the detector, to convert the parallel data output by the plurality of outputs of the detector into serial data,

the parallel to serial converter having an output coupled to the input of the ultrasound console to provide the serial data to the ultrasound console to process into an image.

24. The imaging system of claim 23, wherein:

the first beam splitter is an approximately 50/50 beam splitter; and

the second beam splitter directs more than half of the light energy received from the light source into the sample light beam and less than half of the light energy received from the light source into the reference light beam.

25. The imaging system of claim 24, further comprising a catheter and an optical fiber within the catheter, wherein the second optical path is optically coupled to the optical fiber within the catheter.

26. The imaging system of claim 23, further comprising a focusing lens, wherein the second optical path optically couples the first beam splitter to the focusing lens, to focus the sample light beam onto the sample and to focus the reflected sample light beam.

27. An imaging system comprising:

an ultrasound console having an input;

an interferometer comprising:

a low coherence light source;

a first fiber optic beam splitter;

a first optical fiber optically coupling the light source to the first beam splitter, wherein the first beam splitter splits light received from the light source into a sample light beam and a reference light beam;

an optical circulator having a first port, a second port and a third port, wherein light input to the first port exits the optical circulator from the second port and light entering the second port exits the optical circulator from the third port;

a second optical fiber optically coupling the first beam splitter to the first port of the optical circulator;

a third optical fiber optically coupling the second port of the optical circulator to a sample and optically coupling a reflected sample light beam from the sample to the second port;

a second beam splitter;

a fourth optical fiber optically coupling the third port of the optical circulator to the second beam splitter, wherein the third optical fiber conveys the reflected sample light beam, at least in part, from the third port to the second beam splitter;

a diffraction grating;

a fifth optical fiber optically coupling the first beam splitter to the diffraction grating to convey the reference light beam, at least in part, to the diffraction grating;

the second beam splitter being positioned to receive the diffracted reference light beam from the diffraction grating, wherein the reference light beam and the reflected sample light beam combine in the beam splitter to form a combined light beam; and

a multi-element photo detector positioned to receive the combined beam, the multi-element photo detector having a plurality of parallel outputs; and

the system further comprising a parallel to serial converter comprising a plurality of inputs, each input being coupled to a respective one of the plurality of outputs of the detector, to convert the parallel data output by the plurality of outputs of the detector into serial data,

the parallel to serial converter having an output coupled to the input of the ultrasound console to provide the serial data to the ultrasound console to process into an image.

28. The imaging system of claim **27**, wherein the light received from the light source has an energy and the first beam splitter splits the light into a sample light beam having more than half of the energy of the light and a reference light beam having less than half of the energy of the light.

29. The imaging system of claim **28**, wherein the second beam splitter is an approximately 50/50 beam splitter and the reflected sample light beam and the reference light beam are combined in the second beam splitter to form first and reflected sample light beams, wherein the first combined light beam is received by the first multi element photo detector; and

the interferometer further comprises a second multi-element photo detector positioned to receive a second combined beam from the second beam splitter, the second multi-element photo detector comprising a plurality of parallel outputs coupled to the parallel to serial converter.

30. The imaging system of claim **29**, further comprising a catheter and an optical fiber within the catheter, wherein the third optical fiber is optically coupled to the optical fiber within the catheter.

31. The imaging system of claim **27**, further comprising a catheter and an optical fiber within the catheter, wherein the third optical fiber is optically coupled to the optical fiber within the catheter.

32. The imaging system of claim **27**, further comprising a focusing lens to focus the sample light beam from the third optical fiber onto the sample and to focus the reflected sample light beam into the third optical fiber.

33. An imaging system comprising:

an ultrasound console having a serial input;

an interferometer comprising:

a multi-element photo detector, having a plurality of parallel outputs,

a low coherence light source,

a first beam splitter in communication with the light source to split light from the light source into a first sample light beam to be directed onto a sample and a reference light beam,

a diffraction grating in communication with the first beam splitter to receive the reference light beam from the first beam splitter and to diffract the reference light beam,

a second beam splitter positioned to receive a reflected sample light beam from the sample, the second beam splitter being in communication with the diffraction grating to receive the diffracted reference light beam, wherein the reflected sample light beam and the diffracted reference light beam are combined in the second beam splitter to form a combined light beam, and

a detector positioned to receive the combined light beam from the second beam splitter; and

a parallel to serial converter electrically coupling the plurality of parallel outputs of the multi-element photo detector to the serial input of the ultrasound console, wherein the ultrasound console processes data provided by the interferometer to form an image for display.

34. The imaging system of claim **33**, wherein at least one of the first beam splitter and the second beam splitter is a non 50/50 beam splitter.

35. The imaging system of claim **34**, wherein:

the first beam splitter is an approximately 50/50 beam splitter; and

the second beam splitter directs more than half of the light energy in the reflected sample light beam into the combined beam and directs less than half of the light energy in the reference light beam into the combined beam.

36. The imaging system of claim **35**, wherein the second beam splitter directs substantially more than half of the light energy in the reflected sample light beam into the combined light beam and directs substantially less than half of the light energy in the reference light beam into the combined beam.

37. The imaging system of claim **36**, wherein the diffraction grating is a reflective diffraction grating, a transparent diffraction grating or an acousto optic modulator.

38. The imaging system of claim **34**, wherein the first beam splitter directs more than half of the light energy received from the light source into the sample light beam and less than half of the light energy received from the light source into the reference light beam.

39. The imaging system of claim **38**, further comprising an optical circulator, wherein the sample light beam is directed to the sample through the optical circulator and the reflected sample light beam is directed to the second beam splitter through the optical circulator.

40. The imaging system of claim **39**, wherein the second beam splitter directs substantially more than half of the light energy received from the light source into the sample light beam and substantially less than half of the light energy received from the light source into the reference light beam.

41. The imaging system of claim **40**, wherein the second beam splitter is an approximately 50/50 beam splitter and the reflected sample light beam and the reference light beam are combined in the second beam splitter to form first and second combined light beams, the first light beam being detected by the first detector; and the interferometer further comprises a second detector to detect the second light beam.

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专利名称(译)	用于通过超声控制台处理来自干涉仪的信号的系统和方法		
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申请(专利权)人(译)	CROWLEY罗伯特J. 巴巴托LOUIS J. 奥斯特洛夫斯基ISAAC MODELL MARK D.		
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助理审查员(译)	康诺利PATRICK		
其他公开文献	US20030020922A1		
外部链接	Espacenet USPTO		

摘要(译)

成像系统包括干涉仪和超声控制台，其将来自干涉仪的信号处理成图像以供显示。干涉仪可以包括具有多个并行输出的一个或多个多元件光电检测器。在干涉仪的并行输出和超声控制台的输入之间提供并行到串行转换器，以将并行输出上提供的信号转换成串行信号，以供超声控制台分析。干涉仪可以选择性地耦合到超声控制台，并且系统还可以包括超声设备，该超声设备也可以选择性地耦合到控制台，向用户提供使用干涉仪或超声设备的选项。超声控制台还可以包括两个输入，一个用于干涉仪，另一个用于超声设备。干涉仪和超声装置都可以由导管携带，以插入内部体腔，例如血管。还公开了成像方法。

