



US 20190192116A1

(19) **United States**

(12) **Patent Application Publication**  
**Beckers et al.**

(10) **Pub. No.: US 2019/0192116 A1**  
(43) **Pub. Date: Jun. 27, 2019**

(54) **IMAGING DEVICE WITH ULTRASOUND  
TRANSDUCER ARRAY**

*A61B 8/08* (2006.01)  
*G10K 11/02* (2006.01)

(71) Applicant: **KONINKLIJKE PHILIPS N.V.**,  
EINDHOVEN (NL)

(52) **U.S. Cl.**  
CPC ..... *A61B 8/445* (2013.01); *A61B 8/4494*  
(2013.01); *G10K 11/02* (2013.01); *A61B*  
*8/4281* (2013.01); *A61B 8/488* (2013.01);  
*B06B 1/0292* (2013.01)

(72) Inventors: **Lucas Johannes Anna Maria Beckers**,  
Veldhoven (NL); **Vincent Adrianus**  
**Henneken**, Utrecht (NL)

(73) Assignee: **KONINKLIJKE PHILIPS N.V.**,  
EINDHOVEN (NL)

(57) **ABSTRACT**

(21) Appl. No.: **16/329,048**

(22) PCT Filed: **Aug. 22, 2017**

(86) PCT No.: **PCT/EP2017/071067**

§ 371 (c)(1),  
(2) Date: **Feb. 27, 2019**

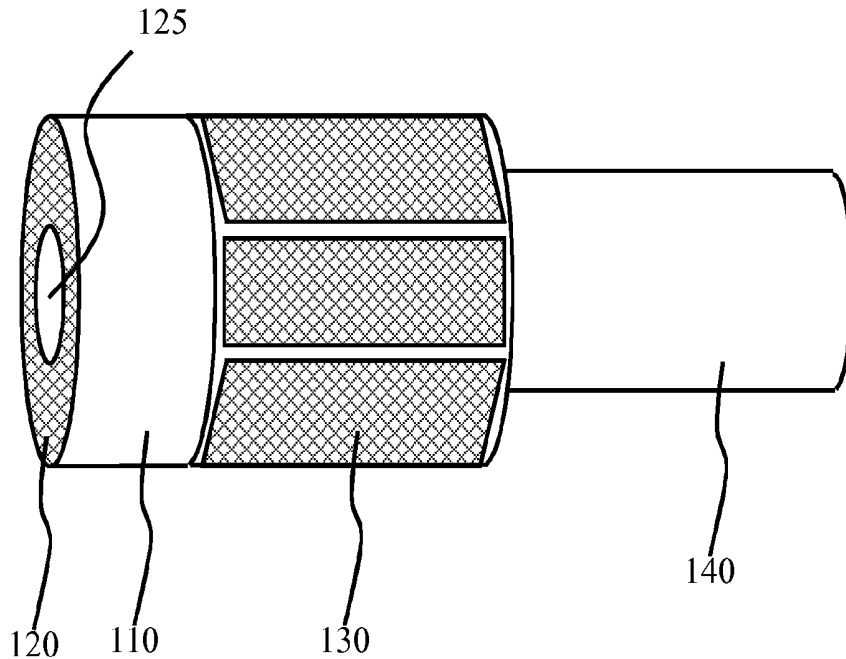
(30) **Foreign Application Priority Data**

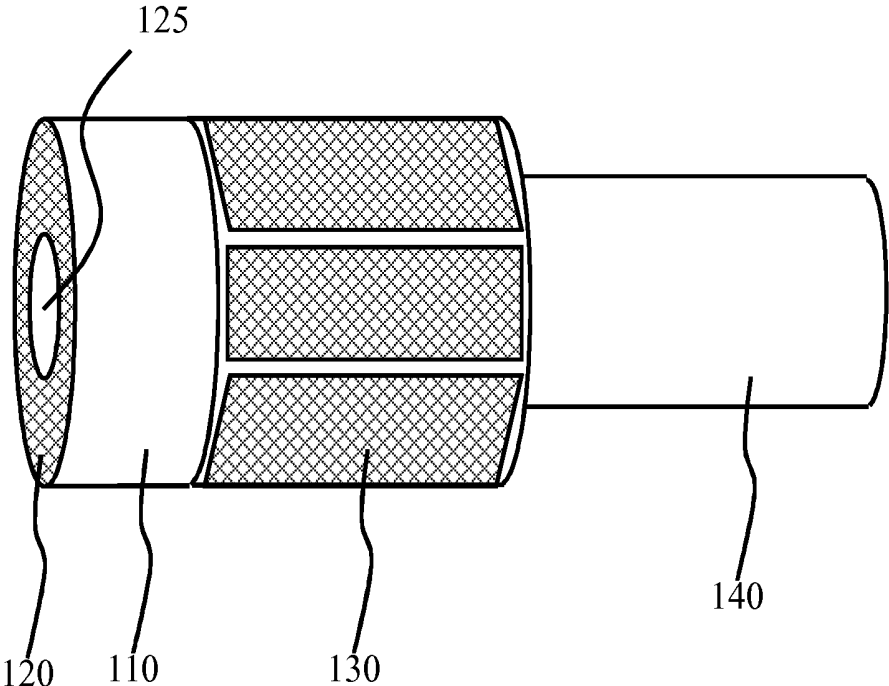
Aug. 30, 2016 (EP) ..... 16186332.9

**Publication Classification**

(51) **Int. Cl.**  
*A61B 8/00* (2006.01)  
*B06B 1/02* (2006.01)

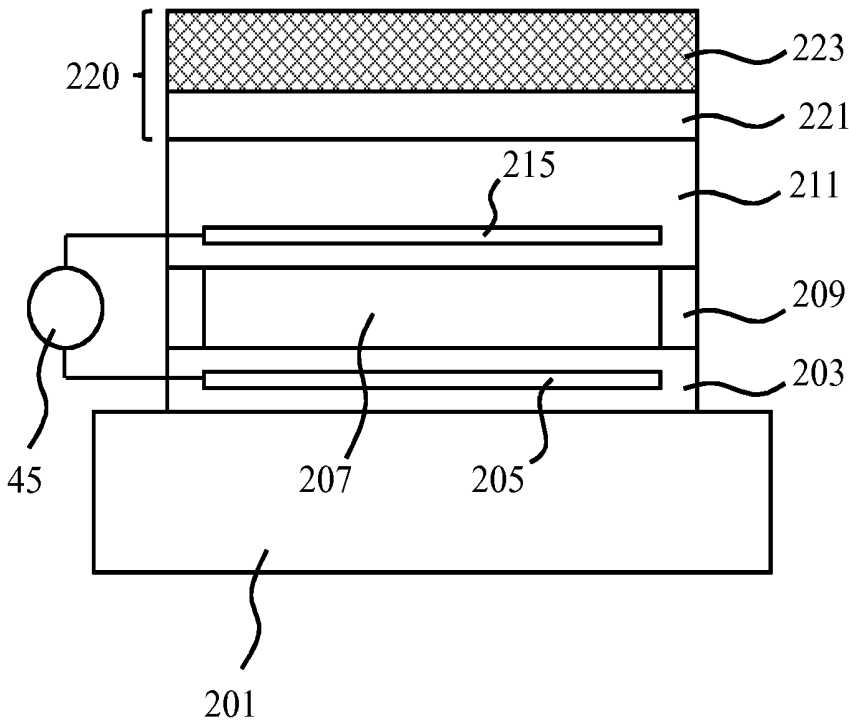
An imaging device (100) is disclosed comprising an ultrasound transducer array (101, 120, 130) having a plurality of ultrasound transducer elements defining an ultrasound emitting surface of the ultrasound transducer array; and an acoustic window (220) on the ultrasound emitting surface, said acoustic window comprising: a first layer (221) of a hydrocarbon elastomer contacting the ultrasound emitting surface, said first layer further containing an antioxidant; and a second layer (223) of a further hydrocarbon elastomer on the first layer, said second layer having a greater Shore A hardness than the first layer. Also disclosed are an ultrasound imaging system (10) comprising such an imaging device, such as catheter (100), and a method (300) of forming an acoustic window (220) on an ultrasound transducer array (101, 120, 130) for such a device (100).





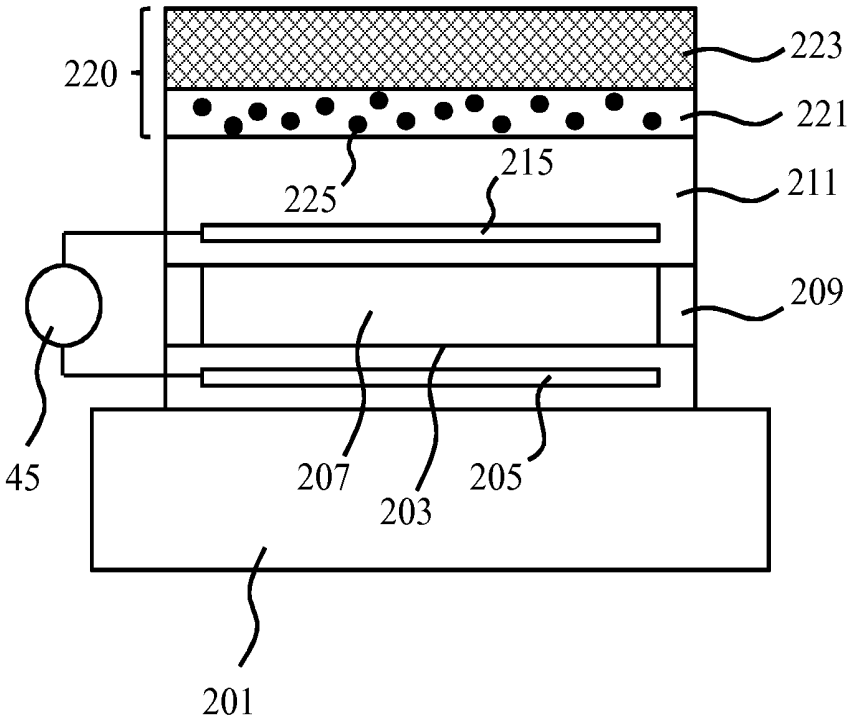
100

**FIG. 1**



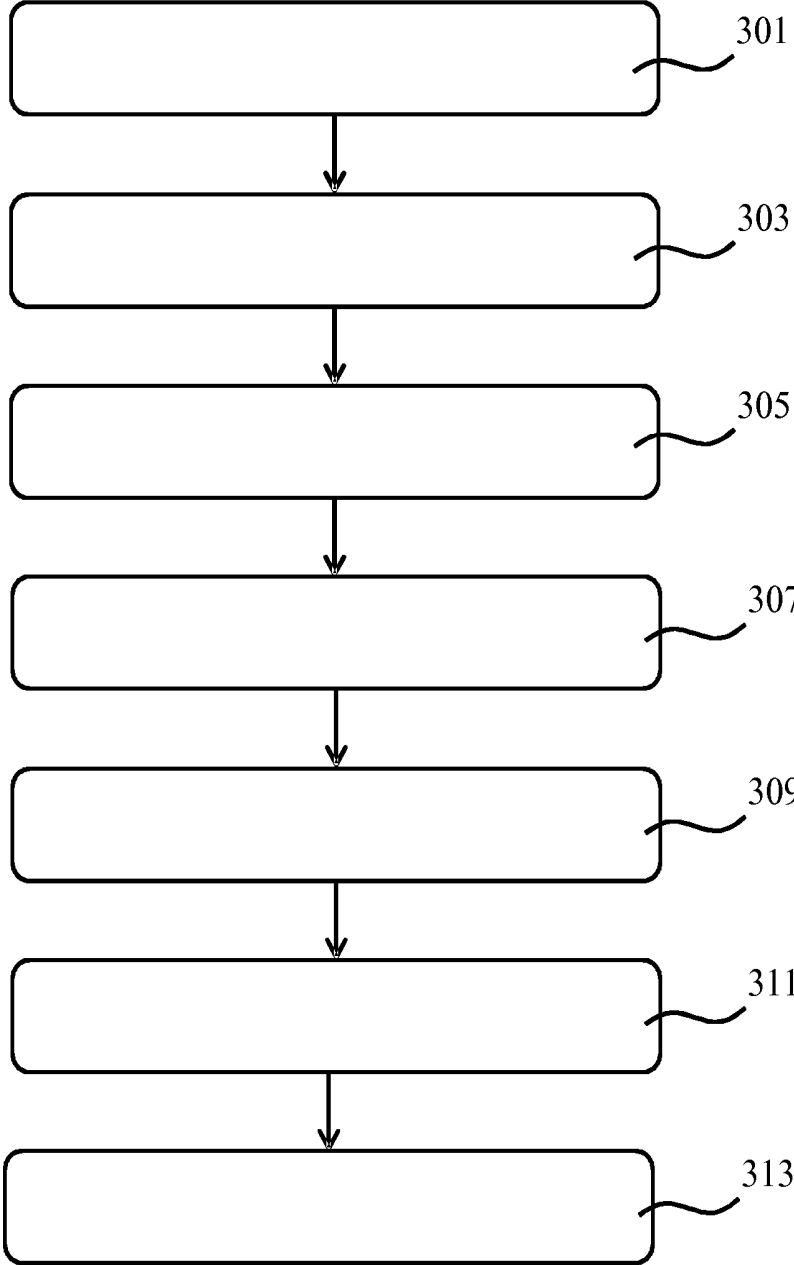
200

**FIG. 2**



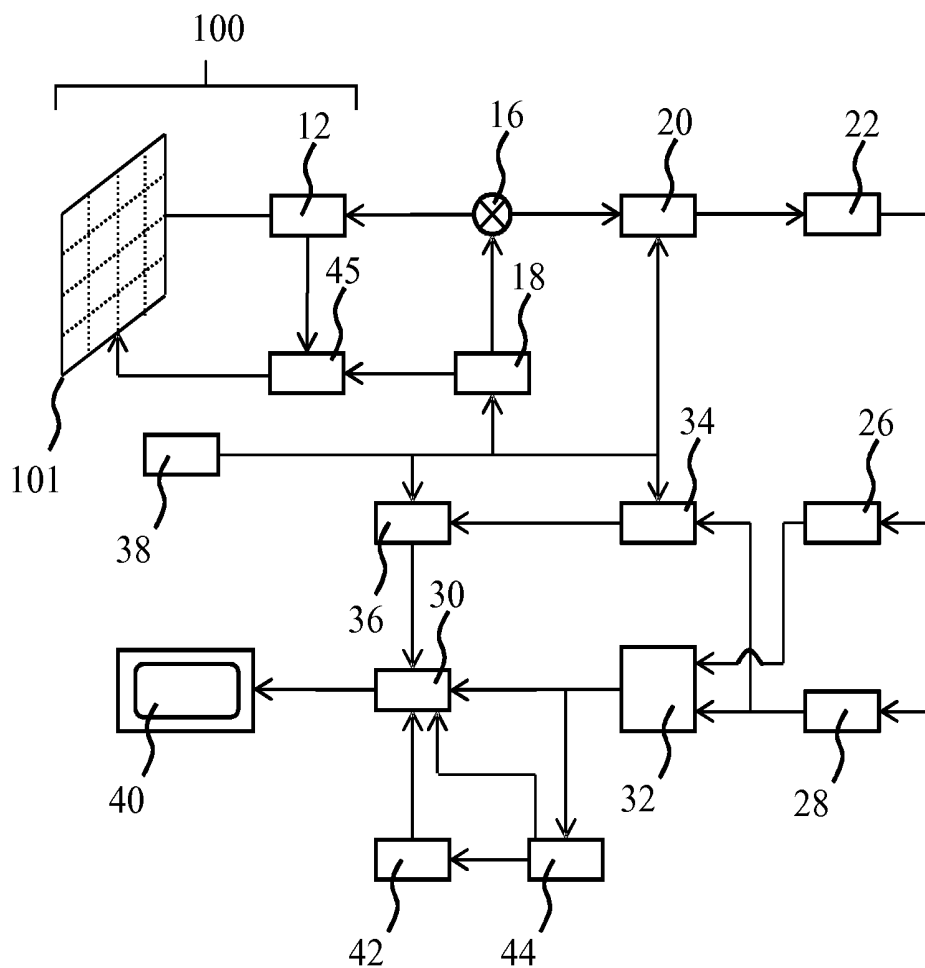
200

**FIG. 3**



300

**FIG. 4**



10

FIG. 5

## IMAGING DEVICE WITH ULTRASOUND TRANSDUCER ARRAY

### FIELD OF THE INVENTION

[0001] The present invention relates to an imaging device comprising an ultrasound transducer array having a plurality of ultrasound transducer elements defining an ultrasound emitting surface of the ultrasound transducer array; and an acoustic window on the ultrasound emitting surface.

[0002] The present invention further relates to an ultrasound imaging system comprising such an imaging device.

[0003] The present invention further relates to a method of forming such an acoustic window on the ultrasound emitting surface of an ultrasound transducer array for such an imaging device.

### BACKGROUND OF THE INVENTION

[0004] Ultrasound imaging is an important diagnostic tool for imaging internals of the patient's body. This is typically achieved using one or more ultrasound transducer elements, typically organised in an ultrasound transducer array, which convert electrical energy into acoustic energy (ultrasound pulses) and convert the received pulse echoes back into electrical energy, which may be processed by a dedicated processing arrangement to convert the received electrical energy into ultrasound images.

[0005] Commonly used ultrasound transducer elements include piezoelectric-based ultrasound transducers (PZT) and capacitive micro-machined ultrasound transducers (CMUTs). These different types of transducers have in common that they require an acoustic matching material, commonly referred to as an acoustic window, between the ultrasound transducer elements and the patient's body in order to improve the acoustic performance of the ultrasound transducer elements by acoustic impedance matching of the emitting surfaces of the ultrasound transducer elements to the patient's body. An example of a CMUT assembly comprising such an acoustic window is disclosed in US 2016/0101437 A1.

[0006] The composition of such an acoustic window for ultrasound transducer arrays, e.g. ultrasound probes, to be applied to the skin of the patient is relatively straightforward, as the acoustic window does not have to meet stringent water barrier and thickness requirements that for instance are required when the ultrasound transducer array has to be operated for a longer period of time (such as monitoring) or within the body of the patient. One such application domain is catheters equipped with ultrasound imaging functionality, e.g. comprising a forward facing and/or side facing ultrasound transducer array. Such catheters must have a small form factor to facilitate penetration of small cavities, e.g. arteries or veins, within the body of the patient. At the same time, the ultrasound transducer arrays deployed with such catheters must be able to withstand the harsh environments, e.g. bodily fluids such as blood, stomach acid, and the like, in which case the acoustic window typically needs to provide additional protection to the ultrasound transducer elements of such an array. Another example the favorable application is ultrasound based patches, which configured for external use via a surface of a subject. These patches (low profile ultrasound probes) are configured to be used for a longer period of time (from hours

to several days) and are desirable to withstand external body fluids such as sweat as well as a longer exposure to an acoustically coupling gel.

[0007] Materials that are commonly used for such imaging devices comprising ultrasound transducer arrays include silicone layers and soft polyurethane layers, as these materials have favourable acoustic properties but have the disadvantage that they are not watertight. To this end, a covering layer of parylene is often added over the silicone or polyurethane layer to make the acoustic window watertight. However, this compromises the acoustic performance of the ultrasound transducer array due to the introduction of reflections and acoustic ringing problems associated with the interface between these two polymer layers.

### SUMMARY OF THE INVENTION

[0008] The present invention seeks to provide a medical imaging device comprising an ultrasound transducer array having thereon a resilient thin acoustic window that is watertight and has improved acoustic characteristics.

[0009] The present invention further seeks to provide an ultrasound imaging system comprising such an imaging device.

[0010] The present invention yet further seeks to provide a method of forming such an acoustic window and the ultrasound transducer array for an imaging device.

[0011] According to an aspect, there is provided an imaging device such as catheter, said device comprising an ultrasound transducer array having a plurality of ultrasound transducer elements defining an ultrasound emitting surface of the ultrasound transducer array; and an acoustic window on the ultrasound emitting surface, said acoustic window comprising a first layer of a hydrocarbon elastomer contacting the ultrasound emitting surface, said first layer further containing an antioxidant; and a second layer of a further hydrocarbon elastomer on the first layer, said second layer having a greater Shore A hardness than the first layer.

[0012] The present invention is based on the insight that hydrocarbon elastomers, e.g. hydrocarbon thermosetting elastomers, are prone to gradual vulcanisation (oxidative cross-linking) through prolonged exposure to UV light or ambient environments containing oxidants, e.g. oxygen or water. Consequently, the inclusion of an antioxidant in a first layer of such a hydrocarbon elastomer of the acoustic window ensures that this first layer maintains its desired softness, which is desired to maximize the acoustic performance of the hydrocarbon elastomer, whilst the vulcanisation of the second layer, i.e. outer layer, of a further hydrocarbon elastomer of the acoustic window provides the desired watertight characteristic of the acoustic window and the consequential hardening of this second layer further provides improved protection of the ultrasound transducer array against accidental damage, e.g. scratching or the like.

[0013] In order to facilitate the selective hardening of the second layer, the second layer may not contain the (i.e. any) antioxidant, such that oxidation (weathering) of the second layer is not suppressed. The further hydrocarbon elastomer in the second layer may be actively cross-linked to accelerate the hardening of the second layer.

[0014] In further embodiments the imaging device is configured for external use via a surface of a subject or internal use within a subject. For external use configuration the imaging device preferably comprises an ultrasound probe or a patch enclosing the ultrasound trans-

ducer array. For internal use configuration the imaging device may comprise a catheter.

[0015] In an embodiment, the first layer has a thickness in a range of 5-10 micron as this is the minimum thickness at which the acoustic window achieves the desired acoustic impedance matching properties. The acoustic window may have a thickness of less than 100 micron and preferably less than 30 micron to make the acoustic window particularly suitable for catheter applications, i.e. to limit the dimensions of the catheter whilst achieving the desired acoustic properties of the acoustic window.

[0016] The hydrocarbon elastomer preferably is the same as the further hydrocarbon elastomer such that the acoustic properties of the first and second layers are closely matched. Polybutadiene is particularly suitable although other hydrocarbon elastomers, e.g. hydrocarbon copolymers, may be contemplated as alternatives to polybutadiene.

[0017] The first layer preferably has a Shore A hardness of less than 50 Shore, preferably less than 10 Shore, when measured with a durometer in accordance with the ASTM D2240 standard. This ensures good compliance with a moving ultrasound emitting surface, e.g. a membrane of a CMUT cell, whilst at the same time providing the first layer with a desirable acoustic impedance.

[0018] The antioxidant may be a phenolic stabilizer such as a stabilizer comprising a sterically hindered phenol head group and an aliphatic, e.g. hydrocarbon, tail, to facilitate blending of the antioxidant in the hydrocarbon elastomer.

[0019] The first layer may contain the antioxidant in an amount of 0.05%-0.5% by weight based on the total weight of the first layer. This amount of the antioxidant is sufficient to effectively suppress oxidation of the hydrocarbon elastomer in the first layer without significantly affecting the desired properties, e.g. acoustic impedance, of the first layer.

[0020] At least the first layer of the acoustic window may further comprise particles embedded in the hydrocarbon elastomer in order to tune the density and the acoustic impedance of the first layer, e.g. to minimize an acoustic impedance mismatch between the first layer and the body tissue to be exposed to ultrasound waves generated with the ultrasound transducer array. Such particles for example may be electrically insulating particles such as ceramic particles. The first layer may comprise the particles in an amount of 4-24% by weight based on the total weight of the first layer in order to tune the acoustic impedance of the first layer to a desired value.

[0021] In accordance with another aspect, there is provided an ultrasound imaging system comprising the imaging device of any of the herein described embodiments such an ultrasound imaging and control circuitry for controlling the ultrasound transducer array. Such an ultrasound imaging system, e.g. an ultrasound diagnostic imaging system, benefits from the inclusion of an imaging device according to an embodiment of the present invention by being able to generate high-resolution ultrasound images owing to the acoustic window on the ultrasound transducer array of the imaging device having favourable acoustic impedance properties as well as excellent mechanical properties.

[0022] According to yet another aspect, there is provided a method of forming an acoustic window on an ultrasound transducer array for an imaging device, the ultrasound transducer array having a plurality of ultrasound transducer elements defining an ultrasound emitting surface of the ultrasound transducer array, the method comprising depos-

iting a first solution of a hydrocarbon elastomer and an antioxidant in an organic solvent on the ultrasound emitting surface; removing the organic solvent to form a first layer of the acoustic window contacting the ultrasound emitting surface, said first layer comprising the hydrocarbon elastomer and the antioxidant; depositing a second solution of a further hydrocarbon elastomer in a further organic solvent on the first layer and removing the further organic solvent to form a second layer of the acoustic window contacting the first layer, wherein the second layer has a greater Shore A hardness than the first layer.

[0023] This method facilitates the provision of ultrasound transducer array of an imaging device having an acoustic window that combines favourable acoustic impedance properties with excellent mechanical properties.

[0024] The method preferably further comprises cross-linking the further hydrocarbon elastomer in the second layer to increase the Shore A hardness of the second layer, such that the increased hardness of the second layer does not have to be the result of weathering of the second layer.

[0025] The solvent and the further organic solvent may be an alkane solvent such as heptane. Such solvents are particularly suitable for dissolving hydrocarbon elastomers and have the further benefit that they can be evaporated at relatively low temperatures due to the low vapour pressures of such solvents, such that the acoustic window may be formed without having to expose the ultrasound transducer array and the acoustic window layers to overly elevated temperatures, which may damage the ultrasound transducer array and/or the acoustic window layers.

[0026] The hydrocarbon elastomer preferably is the same as the further hydrocarbon elastomer. Polybutadiene is particularly suitable as polybutadiene has particularly favourable acoustic properties and may be readily oxidized (vulcanized) to form a second layer of the acoustic window having the desired mechanical and moisture barrier properties.

#### BRIEF DESCRIPTION OF THE DRAWINGS

[0027] Embodiments of the invention are described in more detail and by way of non-limiting examples with reference to the accompanying drawings, wherein:

[0028] FIG. 1 schematically depicts a catheter as an example of an imaging device;

[0029] FIG. 2 schematically depicts an aspect of an imaging device according to an example embodiment;

[0030] FIG. 3 schematically depicts an aspect of an imaging device according to another example embodiment;

[0031] FIG. 4 is a flowchart of a method for forming an acoustic window or the ultrasound transducer array of such an imaging device; and

[0032] FIG. 5 schematically depicts a circuit diagram of an ultrasound imaging system according to an example embodiment.

#### DETAILED DESCRIPTION OF THE EMBODIMENTS

[0033] It should be understood that the Figures are merely schematic and are not drawn to scale. It should also be understood that the same reference numerals are used throughout the Figures to indicate the same or similar parts.

[0034] FIG. 1 schematically depicts an example embodiment of an imaging device: a catheter **100**. The catheter **100**

has a forward facing array **120** of ultrasound transducer elements mounted on the tip **110** of the catheter **100**. The forward facing array **120** for example may be an IC chip carrying the ultrasound transducer elements, which may be mounted on the tip **110** in any suitable manner, e.g. gluing. The forward facing array **120** may include an aperture or channel **125** to facilitate an instrument (not shown) to extend through the tip of the catheter, e.g. for extracting a tissue sample from the patient for biopsy purposes. The catheter **100** may further comprise an arrangement of ultrasound transducer elements **130** wrapped around a side wall of the catheter **100**, thereby facilitating a close to 360° field of ultra-sound vision of the catheter **100**. In some embodiments the catheter can include only the side looking arrangement of the elements **130**. This for instance may be achieved by providing islands or chips **130** carrying one or more ultrasound transducer elements interconnected by a flexible strip or the like that facilitates the wrapping of the respective islands or chips **130** around the catheter side wall. As such flexible arrangements are well-known per se, this will not be explained in further detail for the sake of brevity. The forward facing array **120** and the islands or chips **130** may contain any suitable number and type of ultrasound transducer elements benefiting from an acoustic window according to embodiments of the present invention as will be explained in further detail below. For example, the ultrasound transducer elements may be CMUT elements, PZT elements, and so on. The catheter tip **110** may be connected to a guide wire **140** or the like, to facilitate maneuvering the catheter tip **110** to the desired location within a patient's body.

[0035] It should be understood that embodiments of the present invention are not limited to the depicted example embodiment of the catheter **100**. For example, it is equally feasible for the catheter **100** to only comprise one or more forward facing ultrasound transducer elements or to only comprise one or sideways facing ultrasound transducer elements. Similarly, the aperture or channel **125** may not be present, and so on. Embodiments of the present invention may be applied to any catheter design comprising any number of ultrasound transducer elements carrying an acoustic window according to an embodiment of the present invention.

[0036] In further embodiments the imaging device may be configured for external use via a surface of a subject or internal use within a subject (not shown). In this case the imaging device might include an ultrasound probe (preferably low profile ultrasound probe) comprising an acoustic window **220** coupled to an ultrasound emitting surface of said probe and described in more detail below. FIG. 2 schematically depicts an ultrasound transducer element **200** (here a CMUT cell by way of non-limiting example) as deployed on an imaging device such as a catheter **100** or an ultrasound probe (patch), said element comprising the acoustic window **220** according to an embodiment of the present invention. Such a CMUT cell **200** is typically fabricated on a substrate **201**, such as a silicon wafer. An ultrasound transducer array of an ultrasound imaging system may comprise one or more CMUT cells **200**. The CMUT cells **200** may be either individually activated or in combination with each other. The individual cells **200** can have round, rectangular, hexagon or other peripheral shapes.

[0037] Each CMUT cell **200** has at least a pair of electrodes **205** and **215** separated by a cavity **207**. The cavity **207**

is formed in between a membrane **211** that is suspended over a cell floor **203** formed by the top surface of the substrate **201**. The membrane **211** may be made of one or more layers of electrically insulating materials, e.g. silicon oxide ( $\text{SiO}_x$ ,  $x>1$ ), silicon nitride, low-k dielectric materials and the like. The membrane **211** is flexible, i.e. is adapted to move or vibrate. The membrane **211** may be suspended over the cell floor **203** (i.e. the substrate **201**) through a support structure **209**, which may be made of the same material as the membrane **211**, e.g. by depositing the membrane **211** over a sacrificial material defining the cavity **207** and subsequently removing the sacrificial material to form the cavity **207** surrounded by the membrane **211** including the support structure **209**.

[0038] The electrodes **205**, **215** may be made of any suitable electrically conductive material, such as a metal or metal alloy. The bottom electrodes **205** may be embedded in the floor **203** of the cell **200**, while the top electrode **215** may be embedded in the membrane **211**. The electrode **205** and **215** may be deposited on the cell floor **31** or the membrane **5** as additional layers. The bottom electrode **205** may be insulated on its cavity-facing surface with an additional layer (not pictured). This insulating layer may comprise either one of or a combination of an oxide-nitride-oxide (ONO) dielectric layer, silicon oxide layer, aluminum or hafnium oxide layers, for example. The insulating layer may be formed above the bottom electrode **205** and below the membrane electrode **215**. An ONO-dielectric layer advantageously reduces charge accumulation on the electrodes which leads to device instability, drift and reduction in acoustic output pressure. The cavity **207** may be either air- or gas-filled, or wholly or partially evacuated. Two electrodes **205** and **215** separated by the cavity **207** represent a capacitance.

[0039] An application of electrical signal through a drive circuit **45** coupled to the electrodes **205** and **215** causes a mechanical movement/vibration of the membrane **211**, which results in the change of the capacitance and can be manipulated by integrated circuitry associated with the CMUT cell **200**. An example embodiment of such integrated circuitry will be explained in more detail below. The drive circuit **45** may be implemented as an integrated part of the integrated circuitry. The drive circuit **45** usually comprises an A/C signal source and a D/C voltage source. In a transmit mode of the CMUT cell **200**, the D/C voltage source may be used to bias the membrane **211** with the A/C signal source driving an oscillation of the biased membrane **211** to generate ultrasound signals, e.g. pulses, at the oscillation frequency, as is well-known per se. The A/C component is typically omitted in a receive mode of the CMUT cell **200**, in which the oscillations of the membrane **211** are induced by echoes of previously emitted ultrasound signals, e.g. pulse echoes, by the CMUT cell **200**. In an embodiment, the D/C voltage source may be adapted to bias the membrane **211** into a so-called collapse mode, in which a central portion of the membrane **211** is kept in contact with the cell floor **203** during the oscillations induced with the A/C signal originating from the A/C signal source. As is well-known per se, operation of a CMUT cell **200** in collapse mode may increase the acoustic pressure and the dynamic range of the CMUT cell **200**.

[0040] According to an embodiment of the present invention, the transducer element, here a CMUT cell **200** by way of non-limiting example as previously explained as other

types of transducer elements, e.g. PZT elements, may also be deployed, further comprises an acoustic window **220** preferably having a total thickness of less than 100 micron, more preferably less than 30 micron, in some embodiments, e.g. catheter applications. The acoustic window **220** comprises a first layer **221** contacting the ultrasound emitting surface of the ultrasound transducer element (e.g. the upper surface of the membrane **211** of a CMUT cell **200**) and a second layer **223** on the first layer **221** such that the first layer **221** is sandwiched in between the ultrasound emitting surface and the second layer **223**. The first layer **221** and the second layer **223** both may be formed from the same hydrocarbon elastomer or from different hydrocarbon elastomers preferably having closely matched acoustic properties, e.g. acoustic impedances. Hydrocarbon elastomers, and in particular polybutadiene, may have a density equal or below  $0.95 \text{ g/cm}^3$  and may exhibit a low acoustic energy loss (attenuation) and a suitable acoustic impedance optimization. Acoustic impedance ( $Z$ ) is defined as the product of acoustic propagation velocity ( $v$ ) for acoustic energy (or wave) in a medium and density ( $\rho$ ) of this medium:

$$Z = \rho * v.$$

[0041] Hydrocarbon elastomers may have an acoustic impedance value of above 1.4 MRayl, which is close to soft tissue's impedance of about 1.6 MRayl, such that acoustic losses through acoustic impedance mismatches can be reduced by the deployment of such hydrocarbon elastomers, e.g. polybutadiene. Such elastomers may exhibit an acoustic loss per millimeter for acoustic energy passing therethrough of less than 1.5 dB for a wide range of the acoustic wave frequencies applicable in medical ultrasound, such as in between 2 and 25 MHz, which are typical frequency domains of a wide variety of ultrasound transducer elements including CMUTs and PZTs. Furthermore, such elastomers have a relatively low density and in an uncured state have a hardness value below 50 Shore A, which softness combined with the aforementioned low acoustic wave attenuation characteristics of such elastomers may provide a beneficial effect on the improved acoustic coupling of the ultrasound transducer element (in particular a CMUT vibrating membrane) with the acoustic window layer.

[0042] However, the softness of such hydrocarbon elastomers is less suitable to provide the ultrasound transducer element with mechanical protection and may not provide the ultrasound transducer element with the desired moisture barrier properties. Moreover, many hydrocarbon elastomers, such as in particular polybutadiene, experience hardening over time through (photo-)oxidation causing cross-linking (vulcanization) of the elastomer material when exposed to UV light or oxygen for instance, causing a degradation of the acoustic properties of the hydrocarbon elastomer. At the same time, such vulcanization improves the mechanical robustness and moisture barrier properties of the hydrocarbon elastomer.

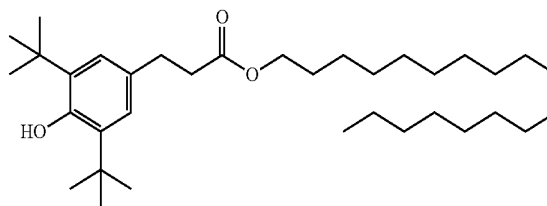
[0043] This insight has been utilized in embodiments of the present invention, in which the first layer **221** of a hydrocarbon elastomer, preferably in uncured form, in the acoustic window **220** further comprises an antioxidant to prevent vulcanization of the first layer **221** such that the first layer **221** retains its desired acoustic properties. In contrast, the second layer **223** of a further hydrocarbon elastomer in the acoustic window **220** is allowed to harden through vulcanization, for example by omitting the antioxidant from

the second layer **223** or alternatively by including the antioxidant in the second layer **223** in such an amount (i.e. a small amount than in the first layer **221**) such that vulcanization of the second layer **223** is not prevented, but instead the rate of vulcanization is controlled by the inclusion of the small amount of antioxidant in the second layer **223**. The hydrocarbon elastomer and the further hydrocarbon elastomer preferably are the same hydrocarbon elastomer as this guarantees the desired acoustic impedance matching. A particularly suitable hydrocarbon elastomer is polybutadiene although hydrocarbon elastomers such as Butyl (isobutylene-isoprene copolymer), ethylene propylene, isoprene, e.g. synthetic cis-isoprene or natural isoprene, may be considered as alternatives to polybutadiene. The first layer **221** preferably has a Shore A hardness of less than 50 Shore A, preferably of less than 10 Shore A, when measured with a durometer in accordance with the ASTM D2240 standard. The second layer **223** preferably has a Shore A hardness in excess of 50 Shore A, preferably in excess of 60 Shore A, when measured with a durometer in accordance with the ASTM D2240 standard.

[0044] In an embodiment, the second layer **223** may be left to naturally vulcanize during use of the imaging device although in an alternative preferred embodiment, the hydrocarbon elastomer in the second layer **223** is actively vulcanized, e.g. using a suitable heat treatment, to obtain a cross-linked hydrocarbon elastomer second layer **223** having the desired mechanical and moisture barrier properties. Moreover, by using the same hydrocarbon elastomer, e.g. polybutadiene, for both layers **221** and **223**, excellent adhesion between the layers **221** and **223** is achieved without the need for an adhesive, which would negatively affect acoustic properties of the acoustic window **220**.

[0045] In an embodiment, the first layer **221** may have a thickness in a range of 5-10 micron ( $\mu\text{m}$ ). Any suitable antioxidant may be included in the first layer **221**. Such antioxidants for hydrocarbon elastomers are well-known per se. For example, a particularly suitable class of antioxidants is so-called phenolic stabilizers, which are primary antioxidants that act as hydrogen donors in the polymeric first layer **221**. Such compounds react with peroxy radicals to form hydroperoxides and prevent the abstraction of hydrogen from the hydrocarbon elastomer backbone, thereby preventing cross-linking of the backbone with other backbones in the polymeric first layer **221**. A non-limiting example of such a phenolic stabilizer is shown in Formula 1:

Formula 1



[0046] This antioxidant is marketed by the BASF Company under the trade name Irganox 1076. Without wishing to be bound by theory, it is believed that the hydrocarbon chain of such a phenolic stabilizer improves mixing of the antioxidant with a hydrocarbon backbone of an elastomer such as polybutadiene, whilst the sterically hindered phenol

group forming a head of the antioxidant molecule acts as a hydrogen donor thereby buffering ambient oxygen. However, it is reiterated for the avoidance of doubt that embodiments of the present invention are not limited to a particular type of phenolic stabilizer or indeed a particular type of antioxidant; any suitable antioxidant may be used in the first layer **221** of the acoustic window **220**. The antioxidant may be present in the first layer **221** in an amount of 0.05%-0.5% by weight based on the total weight of the first layer **221** in some embodiments.

**[0047]** Although hydrocarbon elastomers such as polybutadiene have a particularly suitable acoustic impedance for impedance matching a transducer element with body tissue, in particular soft tissue, as previously explained, it may be desirable to further reduce the acoustic impedance mismatch between the acoustic window **220** and in particular the first layer **221** of the acoustic window **220** and such body tissue. To this end, at least the first layer **221** of the acoustic window **220** may further include particles **225** as schematically depicted in FIG. 3. The particles **225** preferably are made of an electrically insulating material such as a ceramic material having a higher density than the hydrocarbon elastomer such as to increase the total density of the first layer **221**. For example, ceramic particles such as metal oxide ( $ZrO_2$ ,  $Al_2O_3$ ,  $TiO_2$ ,  $Bi_2O_3$ ,  $BaSO_4$ , and so on) particles exhibit electrically insulating properties, which may be advantageous in providing additional electrical insulation to the transducer element electronics. It has been found that the inclusion (embedding) of such particles **225** in the first layer **221** causes minimal additional acoustic losses, in particular when the first particles **225** are included in the first layer **221** in an amount of 4-24% by weight based on the total weight of the first layer **221**, preferably in an amount of 5-20% by weight based on the total weight of the first layer **221**.

**[0048]** The particles **225** preferably have an average size lower than one tenth of the acoustic wavelength of the shortest wave within an operation bandwidth for the selected ultrasound application of the ultrasound transducer element (s) of the catheter **100**. When the average size of the particles **225** becomes larger than the wavelength of the propagating ultrasound wave, this may cause additional scattering of the ultrasound wave in the acoustic window **220**. For example, the particles may have an average size in between 10 nm and 10 micron, in particular in between 10-100 nm or in between 1-10 micron, depending on the operation bandwidth of the ultrasound transducer element(s) of the catheter **100**.

**[0049]** As an example, Table 1 shows the measured changes in acoustic properties of an uncured polybutadiene layer with the introduction of zirconium dioxide ( $ZrO_2$ ) insulating particles having in average diameter of about 2.5 micron and taking a fixed percentage of a total weight of the first layer **221**.

TABLE 1

Changes in the density, acoustic wave velocity, acoustic impedance and attenuation (at frequency of 7 MHz) with an increasing percentage by weight of $ZrO_2$ particles based on the total weight of the polybutadiene layer.				
% $ZrO_2$	Density ( $g/cm^3$ )	Velocity (mm/microsec)	Impedance (MRayl)	Attenuation @7 MHz (dB/mm)
0	0.906	1.570	1.423	0.55
4%	0.937	1.553	1.455	0.75

TABLE 1-continued

Changes in the density, acoustic wave velocity, acoustic impedance and attenuation (at frequency of 7 MHz) with an increasing percentage by weight of $ZrO_2$ particles based on the total weight of the polybutadiene layer.				
% $ZrO_2$	Density ( $g/cm^3$ )	Velocity (mm/microsec)	Impedance (MRayl)	Attenuation @7 MHz (dB/mm)
8%	0.972	1.532	1.489	0.87
16%	1.0405	1.503	1.564	1.05
20%	1.0855	1.469	1.5945	1.25

**[0050]** As can be seen from Table 1, the acoustic impedance of the layer can be tuned towards higher values, e.g. closer to the tissue's acoustic impedance by increasing the total density of the first layer **221** by addition of the particles **225** (here  $ZrO_2$  particles) to the layer **221**, whilst the attenuation of the layer **221** still remains below 1.5 dB/mm, even for the layers comprising 20% by weight of the insulating particles **225** ( $ZrO_2$ ). When the first layer **221** of the acoustic window **220** comprising the antioxidant and the hydrocarbon elastomer with embedded insulating particles **225** has a density equal or above  $0.94 g/cm^3$  and an acoustic impedance equal or above 1.5 MRayl, a direct acoustical coupling of the acoustic window **220** to the ultrasound emitting surface of the ultrasound transducer element, e.g. a membrane **211** of the CMUT cell **200** is provided, thereby obviating the need for an additional coupling medium between the acoustic window **220** and the ultrasound transducer element(s). Moreover, an acoustic impedance equal or above 1.5 MRayl closely matches the acoustic impedance of ultrasonicated body tissue as previously explained.

**[0051]** At this point it is noted that although the acoustic window **220** may be deployed on any type of ultrasound transducer element as previously explained, the use of a soft first layer **221** in such an acoustic window **220** is especially advantageous for CMUT cells **220**, in particular CMUT cells **200** operated in the so-called collapse mode. This is because the relatively light molecular weight of the monomers of the hydrocarbon elastomers, combined with these elastomers' relatively low hardness of preferably below 50 ShoreA may provide an improved acoustic contact between the acoustic window **220** and the membrane **211** adapted to vibrate.

**[0052]** FIG. 4 is a flow chart of a method **300** to form an acoustic window **220** on one or more ultrasound transducer elements such as one or more CMUT cells **200**. The method **300** starts in **301** with the preparation of a first solution of the hydrocarbon elastomer, preferably polybutadiene, in an organic solvent such as an alkane solvent, e.g. pentane, hexane, cyclohexane, heptane, octane, and so on. Heptane is particularly mentioned. The solution may be prepared by dissolving a granulate of pre-polymerized polybutadiene (CB728 T from Lanxess) in the organic solvent. An antioxidant, e.g. a sterically hindered phenolic stabilizer such as Irganox 1076 is added, and optionally insulating particles **225** may be added to the solution to increase the acoustic impedance of the first layer **221** to be formed from this solution as previously explained. The polymeric material acts as a dispersion agent for the particles **225**, such that a liquid mixture of the polymeric material and the insulating particles **225** in the organic solvent is provided. The filler particles **225** in the liquid mixture may increase the hardness of the first layer **221** of the acoustic window **220**. To

counteract this, additional dispersion agents such as fatty acids (a carboxylic acid with an aliphatic chain, which is either saturated or unsaturated) may be added to the liquid mixture, which fatty acids may assist in keeping the average hardness of the first layer **221** at a relatively constant value. The unsaturated chains of fatty acid like oleic acid, linoleic acid and linolenic acid (one, two and respectively three double carbon bonds) can polymerize and bond to the polybutadiene chains. This provides a good dispersion/distribution of particles **225** in the liquid mixture.

**[0053]** Next, the first solution is applied in **303** to the ultrasound emission surface of an ultrasound transducer array **101** comprising one or more ultrasound transducer elements, e.g. by dip coating the ultrasound emission surface with the first solution or by dispensing the first solution on the ultrasound emission surface using well-known dispensing techniques. The thickness of the first solution layer on the ultrasound emission surface may be controlled in case of the dip coating technique by the contact time between the first solution and the ultrasound emission surface.

**[0054]** Next, in **305**, the organic solvent is evaporated from the first solution layer on the ultrasound emission surface during a drying step to form the first layer **221** of the acoustic window **220**. This for example may be achieved by a drying process at an elevated temperature, e.g. about 70° C. This drying step may be terminated once the first layer **221** becomes tacky, to promote adhesion of the second layer **223** to the first layer **221** without requiring separate adhesives.

**[0055]** A second solution of a further hydrocarbon elastomer, which may be the same hydrocarbon elastomer as used in the first solution, e.g. polybutadiene, is prepared in **307**, which second solution may be prepared in the same manner as the first solution using the same constituents apart from the reduction or omission of the antioxidant from the second solution in order to prepare a second layer **223** that can be vulcanized (cross-linked) in order to increase the Shore A hardness of the second layer **223** compared to the first layer **221**. Preferably, the second solution does not contain any antioxidant. In **309**, a layer of the second solution is applied over the partially developed first layer **221**, e.g. through dip coating, dispensing or the like, after which the second solution layer is dried in **311** at a temperature, e.g. 100° C., sufficient to remove the remaining solvent from the partially developed first layer **221** and the second solution layer to form the second layer **223** over the first layer **221**, which second layer **223** may be cured, e.g. cross-linked in **313** (or alternatively during the development step in **311**) to form the acoustic window **220** over the ultrasound transducer array **101**. The ultrasound transducer array **101** may be in situ on the imaging device such as the catheter **100** or may be mounted on this imaging device (catheter **100**) after deposition of the acoustic window **220** on the ultrasound emission surface(s) of the ultrasound transducer array **101**.

**[0056]** It is noted for the avoidance of doubt that the acoustic window forming method **300** as depicted by the flowchart of FIG. **4** is a non-limiting example embodiment of such a method; many variations to this method will be immediately apparent to the skilled person. For instance, the skilled person will immediately realize that the order of the steps depicted in the flowchart of FIG. **4** may be altered without departing from the present invention; for example, the second solution may be prepared prior to or simultane-

ously with the first solution. Also, although the first layer **221** and the second layer **223** are preferably formed on the ultrasound emission surface(s) and the first layer **221** respectively without the use of an adhesive such as glue, it should be understood that in alternative embodiments such adhesives may be applied to increase the adhesive strength between the various layers and surfaces.

**[0057]** FIG. **5** schematically depicts a block diagram of the electronics, i.e. control circuitry, of an ultrasound imaging system **10** according to an example embodiment that may be deployed to interface with an imaging device by controlling the ultrasound transducer array **101** including the acoustic window **220** (for example disposed on a catheter **100**) for the generation of ultrasound waves, e.g. ultrasound pulses, and reception of ultrasound echoes, e.g. pulse echoes, e.g. for diagnostic imaging purposes. The ultrasound transducer array(s) **101** of the imaging device may be coupled to a microbeam former **12**, which may be located within said imaging device, e.g. in the ultrasound transducer array **101** or on an interface, e.g. a PCB between the ultrasound transducer array **101** and a coaxial wire connecting the ultrasound transducer array **101** to the electronics, in some embodiments. The microbeam former **12** controls transmission and reception of signals by the one or more ultrasound transducer cells of the ultrasound transducer array **101**. Microbeam formers are capable of at least partial beam forming of the signals received by groups or “patches” of transducer element tiles for instance as described in U.S. Pat. No. 5,997,479 (Savord et al.), U.S. Pat. No. 6,013,032 (Savord), and U.S. Pat. No. 6,623,432 (Powers et al.)

**[0058]** The microbeam former **12** may be coupled by a probe cable, e.g. coaxial wire, to a terminal, e.g. a user console device or the like, comprising a transmit/receive (T/R) switch **16** which switches between transmission and reception modes and protects the main beam former **20** from high energy transmit signals when a microbeam former is not present or used and the ultrasound transducer array **101** is operated directly by the main system beam former **20**. The transmission of ultrasonic beams from the ultrasound transducer array **101** under control of the microbeam former **12** may be directed by a transducer controller **18** coupled to the microbeam former by the T/R switch **16** and the main system beam former **20**, which receives input from the user's operation of the user interface **10** through control panel **38**. One of the functions controlled by the transducer controller **18** is the direction in which beams are steered and focused. Beams may be steered straight ahead from (orthogonal to) the ultrasound transducer array **101**, or at different angles for a wider field of view. The transducer controller **18** may be coupled to control the aforementioned drive circuit **45** for the ultrasound transducer array **101**. For instance, the drive circuit **45** may set the DC and AC bias voltage(s) that are applied to CMUT elements of a CMUT array, e.g. to operate the CMUT elements in collapse mode, as is well-known per se, in case of a CMUT-based ultrasound transducer array **101**. The transducer controller **18** may be further adapted to control the drive circuit **45** such as to switch the ultrasound transducer elements to a low-power mode, e.g. in response to a temperature sensor signal indicative of the ultrasound transducer elements reaching a critical temperature.

**[0059]** The partially beam-formed signals produced by the microbeam former **12** may be forwarded to the main beam former **20** where partially beam-formed signals from indi-

vidual patches of ultrasound transducer elements are combined into a fully beam-formed signal. For example, the main beam former **20** may have 128 channels, each of which receives a partially beam-formed signal from a patch of dozens or hundreds of ultrasound transducer elements and/or from clusters of such ultrasound transducer elements, e.g. from ultrasound transducer tiles carrying a plurality of such ultrasound transducer elements. In this way the signals received by thousands of transducer elements of an ultrasound transducer array **101** can contribute efficiently to a single beam-formed signal.

**[0060]** The beam-formed signals are coupled to a signal processor **22**. The signal processor **22** can process the received echo signals in various ways, such as bandpass filtering, decimation, I and Q component separation, and harmonic signal separation which acts to separate linear and nonlinear signals so as to enable the identification of nonlinear (higher harmonics of the fundamental frequency) echo signals returned from tissue and microbubbles.

**[0061]** The signal processor **22** optionally may perform additional signal enhancement such as speckle reduction, signal compounding, and noise elimination. The bandpass filter in the signal processor **22** may be a tracking filter, with its passband sliding from a higher frequency band to a lower frequency band as echo signals are received from increasing depths, thereby rejecting the noise at higher frequencies from greater depths where these frequencies are devoid of anatomical information.

**[0062]** The processed signals may be forwarded to a B-mode processor **26** and optionally to a Doppler processor **28**. The B-mode processor **26** employs detection of an amplitude of the received ultrasound signal for the imaging of structures in the body such as the tissue of organs and vessels in the body. B-mode images of structure of the body may be formed in either the harmonic image mode or the fundamental image mode or a combination of both for instance as described in U.S. Pat. No. 6,283,919 (Roundhill et al.) and U.S. Pat. No. 6,458,083 (Jago et al.)

**[0063]** The Doppler processor **28**, if present, processes temporally distinct signals from tissue movement and blood flow for the detection of the motion of substances, such as the flow of blood cells in the image field. The Doppler processor typically includes a wall filter with parameters which may be set to pass and/or reject echoes returned from selected types of materials in the body. For instance, the wall filter can be set to have a passband characteristic which passes signal of relatively low amplitude from higher velocity materials while rejecting relatively strong signals from lower or zero velocity material.

**[0064]** This passband characteristic will pass signals from flowing blood while rejecting signals from nearby stationary or slowly moving objects such as the wall of the heart. An inverse characteristic would pass signals from moving tissue of the heart while rejecting blood flow signals for what is referred to as tissue Doppler imaging, detecting and depicting the motion of tissue. The Doppler processor may receive and process a sequence of temporally discrete echo signals from different points in an image field, the sequence of echoes from a particular point referred to as an ensemble. An ensemble of echoes received in rapid succession over a relatively short interval can be used to estimate the Doppler shift frequency of flowing blood, with the correspondence of the Doppler frequency to velocity indicating the blood flow velocity. An ensemble of echoes received over a longer

period of time is used to estimate the velocity of slower flowing blood or slowly moving tissue.

**[0065]** The structural and motion signals produced by the B-mode (and Doppler) processor(s) are coupled to a scan converter **32** and a multiplanar reformatter **44**. The scan converter **32** arranges the echo signals in the spatial relationship from which they were received in a desired image format. For instance, the scan converter may arrange the echo signal into a two dimensional (2D) sector-shaped format, or a pyramidal three dimensional (3D) image.

**[0066]** The scan converter can overlay a B-mode structural image with colors corresponding to motion at points in the image field with their Doppler-estimated velocities to produce a color Doppler image which depicts the motion of tissue and blood flow in the image field. The multiplanar reformatter **44** will convert echoes which are received from points in a common plane in a volumetric region of the body into an ultrasonic image of that plane, for instance as described in U.S. Pat. No. 6,443,896 (Detmer). A volume renderer **42** converts the echo signals of a 3D data set into a projected 3D image as viewed from a given reference point as described in U.S. Pat. No. 6,530,885 (Entrekin et al.)

**[0067]** The 2D or 3D images are coupled from the scan converter **32**, multiplanar reformatter **44**, and volume renderer **42** to an image processor **30** for further enhancement, buffering and temporary storage for display on an image display **40**. In addition to being used for imaging, the blood flow values produced by the Doppler processor **28** and tissue structure information produced by the B-mode processor **26** are coupled to a quantification processor **34**. The quantification processor produces measures of different flow conditions such as the volume rate of blood flow as well as structural measurements such as the sizes of organs and gestational age. The quantification processor may receive input from the user control panel **38**, such as the point in the anatomy of an image where a measurement is to be made.

**[0068]** Output data from the quantification processor is coupled to a graphics processor **36** for the reproduction of measurement graphics and values with the image on the display **40**. The graphics processor **36** can also generate graphic overlays for display with the ultrasound images. These graphic overlays can contain standard identifying information such as patient name, date and time of the image, imaging parameters, and the like. For these purposes the graphics processor receives input from the control panel **38**, such as patient name.

**[0069]** The user interface is also coupled to the transmit controller **18** to control the generation of ultrasound signals from the ultrasound transducer array **101** and hence the images produced by the transducer array and the ultrasound system. The user interface is also coupled to the multiplanar reformatter **44** for selection and control of the planes of multiple multiplanar reformatted (MPR) images which may be used to perform quantified measures in the image field of the MPR images.

**[0070]** As will be understood by the skilled person, the above embodiment of an ultrasonic (diagnostic) imaging system **10** is intended to give a non-limiting example of such an ultrasonic (diagnostic) imaging system. The skilled person will immediately realize that several variations in the architecture of the ultrasonic imaging system **10** are feasible without departing from the teachings of the present invention. For instance, as also indicated in the above embodiment, the microbeam former **12** and/or the Doppler proces-

sor **28** may be omitted, the ultrasound probe **100** may not have 3D imaging capabilities and so on. Other variations will be apparent to the skilled person.

[0071] At this point, it is noted that although the acoustic window **220** according to embodiments of the present invention has particular benefits when applied to an ultrasound transducer array of a catheter **100**, such an acoustic window **220** may be equally applied to ultrasound transducer arrays in other applications, e.g. stand-alone ultrasound transducer arrays such as ultrasound probes to be applied to the skin of a patient. It will be readily understood that in such embodiments, certain embodiments preferred in the context of catheters, such as the overall thickness of the acoustic window **220**, may not necessarily be preferred in such other application domains. Specifically, for a stand-alone ultrasound transducer array (forming a part of the imaging device configured for external use, for example), the acoustic window **220** may have a thickness in excess of **100** micron as in such application domains the thickness is not particularly limited by the application domain (contrary to catheter applications, in which the thickness limitations typically are applicable to limit the overall dimensions of the catheter as previously explained).

[0072] It should be noted that the above-mentioned embodiments illustrate rather than limit the invention, and that those skilled in the art will be able to design many alternative embodiments without departing from the scope of the appended claims. In the claims, any reference signs placed between parentheses shall not be construed as limiting the claim. The word “comprising” does not exclude the presence of elements or steps other than those listed in a claim. The word “a” or “an” preceding an element does not exclude the presence of a plurality of such elements. The invention can be implemented by means of hardware comprising several distinct elements. In the device claim enumerating several means, several of these means can be embodied by one and the same item of hardware. The mere fact that certain measures are recited in mutually different dependent claims does not indicate that a combination of these measures cannot be used to advantage.

1. A imaging device comprising:

an ultrasound transducer array having a plurality of ultrasound transducer elements defining an ultrasound emitting surface of the ultrasound transducer array; and

an acoustic window coupled to the ultrasound emitting surface, said acoustic window comprising:

a first layer contacting the ultrasound emitting surface, said first layer comprising a hydrocarbon elastomer and an antioxidant; and

a second layer contacting the first layer and comprising a further hydrocarbon elastomer, wherein the second layer has a greater Shore A hardness than the first layer and does not contain the antioxidant; and wherein the hydrocarbon elastomer and the further hydrocarbon elastomer are the same hydrocarbon elastomer and the hydrocarbon elastomer in the second layer is at least partially cross-linked.

2. (canceled)

3. (canceled)

4. The imaging device of claim **1** configured for external use via a surface of a subject, preferably said device comprising an ultrasound probe enclosing the ultrasound transducer array.

5. The imaging device of claim **1** configured for internal use within a subject, wherein said device comprises a catheter.

6. The imaging device of claim **5**, wherein the first layer has a thickness in a range of 5-10 micron and/or the acoustic window has a thickness of less than 100 micron, preferably less than 30 micron.

7. (canceled)

8. The imaging device of claim **1**, wherein the hydrocarbon elastomer is polybutadiene.

9. The imaging device of claim **1**, wherein the first layer has a Shore A hardness of less than 50 Shore, preferably less than 10 Shore, when measured with a durometer in accordance with the ASTM D2240 standard.

10. The imaging device of claim **1**, wherein the antioxidant is a phenolic stabilizer.

11. The imaging device of claim **1**, wherein the first layer contains the antioxidant in an amount of 0.05%-0.5% by weight based on the total weight of the first layer.

12. The imaging device of claim **1**, wherein at least the first layer of the acoustic window further comprises particles embedded in the hydrocarbon elastomer, preferably wherein the particles are insulating particles such as ceramic particles.

13. The imaging device of claim **12**, wherein the first layer comprises the particles in an amount of 4-24% by weight based on the total weight of the first layer.

14. An ultrasound imaging system comprising the imaging device of claim **1** and control circuitry for controlling the ultrasound transducer array of said imaging device.

15. A method of forming an acoustic window on an ultrasound transducer array for a imaging device, the ultrasound transducer array comprising a plurality of ultrasound transducer elements that define an ultrasound emitting surface of the ultrasound transducer array, the method comprising:

depositing a first solution that comprises a hydrocarbon elastomer and an antioxidant in an organic solvent on the ultrasound emitting surface;

removing the organic solvent to form a first layer of the acoustic window contacting the ultrasound emitting surface, said first layer comprising the hydrocarbon elastomer and the antioxidant;

depositing a second solution comprising a further hydrocarbon elastomer in a further organic solvent on the first layer;

removing the further organic solvent to form a second layer of the acoustic window contacting the first layer, wherein the second layer comprises a greater Shore A hardness than the first layer;

at least partially cross-linking the further hydrocarbon elastomer in the second layer to increase the Shore A hardness of the second layer;

wherein the hydrocarbon elastomer is the same as the further hydrocarbon elastomer.

16. (canceled)

17. The method of **15**, wherein the hydrocarbon elastomer is the same as the further hydrocarbon elastomer, preferably wherein the hydrocarbon elastomer is polybutadiene.

\* \* \* \* \*

专利名称(译)	具有超声换能器阵列的成像装置		
公开(公告)号	<a href="#">US20190192116A1</a>	公开(公告)日	2019-06-27
申请号	US16/329048	申请日	2017-08-22
[标]申请(专利权)人(译)	皇家飞利浦电子股份有限公司		
申请(专利权)人(译)	皇家飞利浦N.V.		
当前申请(专利权)人(译)	皇家飞利浦N.V.		
[标]发明人	BECKERS LUCAS JOHANNES ANNA MARIA HENNEKEN VINCENT ADRIANUS		
发明人	BECKERS, LUCAS JOHANNES ANNA MARIA HENNEKEN, VINCENT ADRIANUS		
IPC分类号	A61B8/00 B06B1/02 A61B8/08 G10K11/02		
CPC分类号	A61B8/445 A61B8/4494 B06B1/0292 A61B8/4281 A61B8/488 G10K11/02		
优先权	2016186332 2016-08-30 EP		
外部链接	<a href="#">Espacenet</a> <a href="#">USPTO</a>		

摘要(译)

公开了一种成像装置 ( 100 ) , 其包括超声换能器阵列 ( 101,120,130 ) , 其具有限定超声换能器的超声发射表面的多个超声换能器元件。阵列;超声发射表面上的声窗 ( 220 ) , 所述声窗包括:接触超声发射表面的烃弹性的第一层 ( 221 ) , 所述第一层进一步含有抗氧化剂的层;在第一层上具有另外的烃弹性的第二层 ( 223 ) , 所述第二层具有比第一层更大的肖氏A硬度。还公开了一种超声成像系统 ( 10 ) , 其包括这样的成像装置, 例如导管 ( 100 ) 和方法 ( 300 ) 在超声换能器阵列 ( 101,120,130 ) 上为这样的装置 ( 100 ) 形成声窗 ( 220 ) 。

