



US007850611B2

(12) **United States Patent**
Davies et al.

(10) **Patent No.:** US 7,850,611 B2
(45) **Date of Patent:** Dec. 14, 2010

(54) **SYSTEM AND METHODS FOR IMPROVED
ULTRASOUND IMAGING**

5,570,691 A * 11/1996 Wright et al. 600/447

(75) Inventors: **Timothy J. Davies**, Calgary (CA);
Richard Evans, Bristol (GB)

(Continued)

(73) Assignee: **InnerVision Medical Technologies Inc.**,
Calgary (CA)

FOREIGN PATENT DOCUMENTS

EP 0 812 005 A2 12/1997

(*) Notice: Subject to any disclaimer, the term of this
patent is extended or adjusted under 35
U.S.C. 154(b) by 1478 days.

(21) Appl. No.: **10/945,459**

(22) Filed: **Sep. 20, 2004**

(65) **Prior Publication Data**

US 2006/0064015 A1 Mar. 23, 2006

(51) **Int. Cl.**
A61B 8/00 (2006.01)

(52) **U.S. Cl.** **600/447**; 600/437; 600/441;
600/443; 73/596; 73/628

(58) **Field of Classification Search** **600/437**,
600/439, 440, 441, 443, 444, 447, 459, 472;
73/596, 602, 606, 607, 618-629, 632, 633,
73/641

See application file for complete search history.

(56) **References Cited**

U.S. PATENT DOCUMENTS

3,895,381 A 7/1975 Kock
4,325,257 A 4/1982 Kino et al.
4,452,084 A * 6/1984 Taenzer 73/609
4,669,482 A * 6/1987 Ophir 600/449
4,817,434 A 4/1989 Anderson
5,161,536 A * 11/1992 Vilkomerson et al. 600/443
5,269,309 A * 12/1993 Fort et al. 600/447
5,299,576 A 4/1994 Shiba
5,345,426 A * 9/1994 Lipschutz 367/103
5,465,722 A 11/1995 Fort et al.
5,526,815 A * 6/1996 Granz et al. 600/439
5,558,092 A * 9/1996 Unger et al. 600/439

Morten H. Pedersen, Kim L. Gammelmark, and Jorgen A. Jensen;
Preliminary In-Vivo Evaluation of Convex Array Synthetic Aperture
Imaging; SPIE 2004.

(Continued)

Primary Examiner—Ruth S Smith

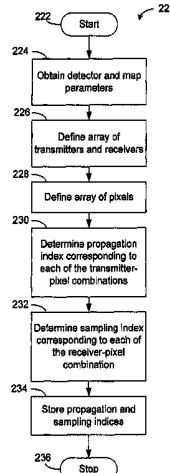
Assistant Examiner—Mark Remaly

(74) *Attorney, Agent, or Firm*—Oyen Wiggs Green & Mutala
LLP

(57) **ABSTRACT**

Systems and methods are disclosed for improving the resolution and quality of an image formed by signals from an array of receivers. Multiple receivers introduce variations in arrival times that can be less than the period of an operating signal, and also less than the period associated with a sampling operation. Thus, multiple receivers allow sampling of fine features of reflected signals that would be considered beyond the resolution associated with the operating signal. Use of multiple receivers also provides an effective sampling rate that is greater than the sampling rate of an individual receiver. Similar advantages can be obtained using multiple transmitters. Such advantageous features can be used to obtain high resolution images of objects in a medium in applications such as ultrasound imaging.

11 Claims, 36 Drawing Sheets



U.S. PATENT DOCUMENTS

5,628,320 A * 5/1997 Teo 600/443
 5,920,285 A 7/1999 Benjamin
 5,969,661 A 10/1999 Benjamin
 6,007,499 A * 12/1999 Martin et al. 601/3
 6,049,509 A * 4/2000 Sonneland et al. 367/49
 6,050,943 A * 4/2000 Slayton et al. 600/439
 6,135,960 A * 10/2000 Holmberg 600/447
 6,166,384 A * 12/2000 Dentinger et al. 250/370.09
 6,231,511 B1 * 5/2001 Bae 600/447
 6,264,609 B1 * 7/2001 Herrington et al. 600/443
 6,436,046 B1 * 8/2002 Napolitano et al. 600/447
 6,526,163 B1 2/2003 Halmann et al.
 6,547,732 B2 * 4/2003 Jago 600/437
 6,672,165 B2 * 1/2004 Rather et al. 73/603
 6,692,450 B1 * 2/2004 Coleman 601/3
 6,719,693 B2 * 4/2004 Richard 600/437
 2002/0065466 A1 * 5/2002 Rather et al. 600/447

FOREIGN PATENT DOCUMENTS

EP 0812005 A2 * 12/1997
 EP 0812005 A2 * 12/1997
 FR 2 851 662 8/2004

OTHER PUBLICATIONS

William D. Richard, A Scalable Architecture For Real-Time Synthetic-Focus Imaging, Ultrasonic Imaging 25, pp. 151-161, 2003.
 Mark A. Franklin, Abhijit Mahajan and R. Martin Arthur; Parallel Implementations of an Ultrasonic Image Generation Algorithm using MPI; Parallel and Distributed Computing and Systems, pp. 589-596, Nov. 3-6, 1999.
 Stephen W. Smith, Henry G. Pavly, Jr., and Olaf T. von Ramm; High-Speed Ultrasound Volumetric Imaging System—Part I: Transducer Design and Beam Steering; IEEE Transactions on Ultrasonics, Ferroelectrics, and Frequency Control, vol. 38, No. 2, pp. 100-108, Mar. 1991.
 Peter Cheesman, Bob Kanefsky, Richard Kraft, John Stutz and Robin Hanson; Super-Resolved Surface Reconstruction from Multiple Images; NASA Ames Research Center, Dec. 14, 1994.
 Jorgen Arendt Jensen, Ole Holm, Lars Joost Jensen, Henrik Bendsen, Henrik Moller Pedersen, Kent Salomonsen, Johnny Hansen and Svetoslav Nikolov; Experimental Ultrasound System for Real-Time Synthetic Imaging; IEEE International Ultrasonics Symposium, Lake Tahoe, 1999.
 Yiming Pi, Hui Long and Shunji Huang; A SAR Parallel Processing Algorithm and its Implementation; Conference Proceedings FIEOS 2002.
 Donald Bailey; Image Resolution Improvement from Multiple Images; Massey University, available online at www.poly.edu/Podium/eef2001.cfm, Nov. 2001.
 Steven R. Broadstone and R. Martin Arthur; An Approach to Real-Time Reflection Tomography Using the Complete Dataset; pp. 829-831, 1986 Ultrasonics symposium.
 Catherine H. Frazier and William D. O'Brien, Jr.; Synthetic Aperture Techniques with a Virtual Source Element; IEEE Transactions on Ultrasonics, vol. 45, No. 1, pp. 196-207, Jan. 1998.
 D.K. Peterson and Gordon S. Kino; Real-Time Digital Image Reconstruction; A Description of Imaging Hardware and an Analysis of Quantization Errors; IEEE Transactions on Sonics and Ultrasonics, vol. SU-31, No. 4, pp. 337-351, Jul. 1984.
 P.D. Corl, P.M. Grant and G.S. Kino; A Digital Synthetic Focus Acoustic Imaging System for NDE; IEEE Ultrasonics Symposium Proceedings; pp. 263-268, 1978.
 Svetoslav I. Nikolov, Jorgen A. Jensen, Remi Dufait and Armin Schoisswohl; Three-Dimensional Real-Time Synthetic Aperture Imaging Using a Rotating Phased Array Transducer; IEEE International Ultrasonics Symposium, 2002.
 Mark A. Franklin, Abhijit Mahajan, and R. Martin Arthur; Parallel Implementations of 3D Synthetic-Focus Ultrasonic Image Generation Using MPI; Parallel and Distributed Computing and Systems; vol. I, pp. 239-246, Nov. 6-9, 2000.
 Daryl G. Bechner and R. Martin Arthur; Generation of Synthetic-Focus Images from Pulse-Echo Ultrasound Using Difference Equations; IEEE Transactions on Medical Imaging, vol. 15, No. 5, pp. 665-672, Oct. 1996.
 William D. Richard and R. Martin Arthur; Real-Time Ultrasonic Scan Conversion via Linear Interpolation of Oversampled Vectors; Ultrasonic Imaging 16, 109-123, 1994.
 An Introduction to the Sampling Theorem; National Semiconductor Application Note 236, Jan. 1980.
 Samuel H. Gray; The Bleeding Edge of Seismic Imaging; CSEG Recorder, Dec. 2003.
 Steven D. Glaser and Mi Kyong Hand; Imaging of Rock Fractures with Low-Frequency Ultrasonic Reflection/Diffraction; American Society for Testing Materials, Geotechnical Testing Journal, vol. 21, No. 4, pp. 317-327, Dec. 1998.
 Samuel H. Gray; Nuts and Bolts of Beam Migration; CSEG National Convention 2004.
 Mark A. Haun; Douglas L. Jones, and William D. O'Brien, Jr; Adaptive Focusing Through Layered Media Using the Geophysical "Time Migration" Concept; Proc. Intl. Ultrasonics Symposium, Munich, Germany, Oct. 8-11, 2002.
 Improved Resolution in Infrared Imaging Using Randomly Shifted Images, available online at <http://www.ph.tn.tudelft.nl/~cris/MastersProject.html>, Nov. 1998.
 George Papanicolaou; Interferometric Imaging in Clutter II; ARO/DARPA MURI, Aug. 15, 2003.
 Jorgen Arendt Jensen; Ultrasound Imaging and its Modeling; 84 Imaging of Complex Media with Acoustic and Seismic Waves, pp. 135-165, 2002.
 Olaf T. Von Ramm, Stephen W. Smith, and Henry G. Pavly, Jr.; High Speed Ultrasound Volumetric Imaging System—Part II: Parallel Processing and Image Display; IEEE Transactions on Ultrasonics, Ferroelectrics, and Frequency Control, vol. 38, No. 2, pp. 109-115, Mar. 1991.
 John E. Greivenkamp, Sub-Nyquist interferometry, Dec. 15, 1997, vol. 26, No. 24, Applied Optics, Rochester, New York.
 Lyons RG; Understanding Digital Signal Processing, 2nd ed. (2004). Section 2.3.
 International Search Report for PCT/IB2005/003147, filed Mar. 8, 2005.

* cited by examiner

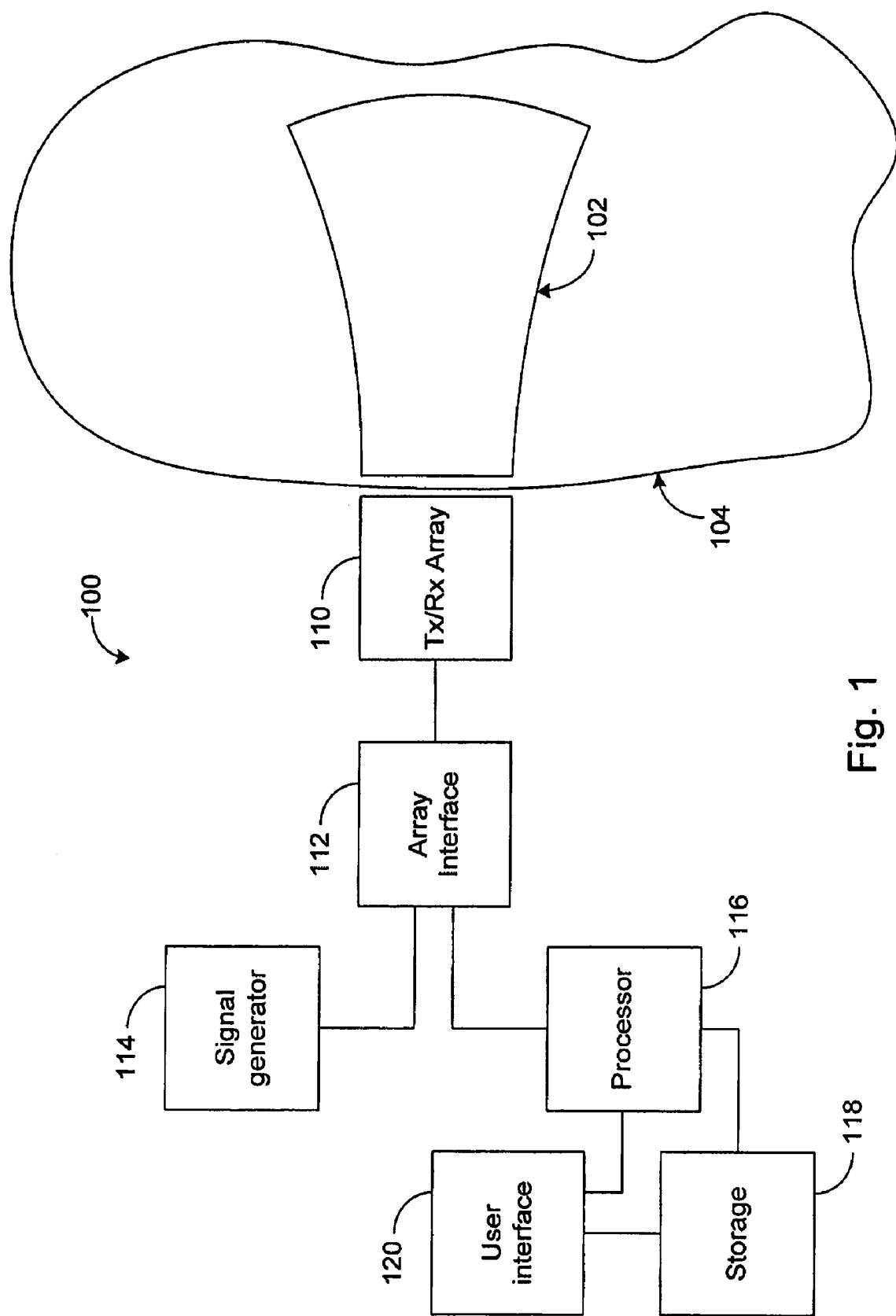


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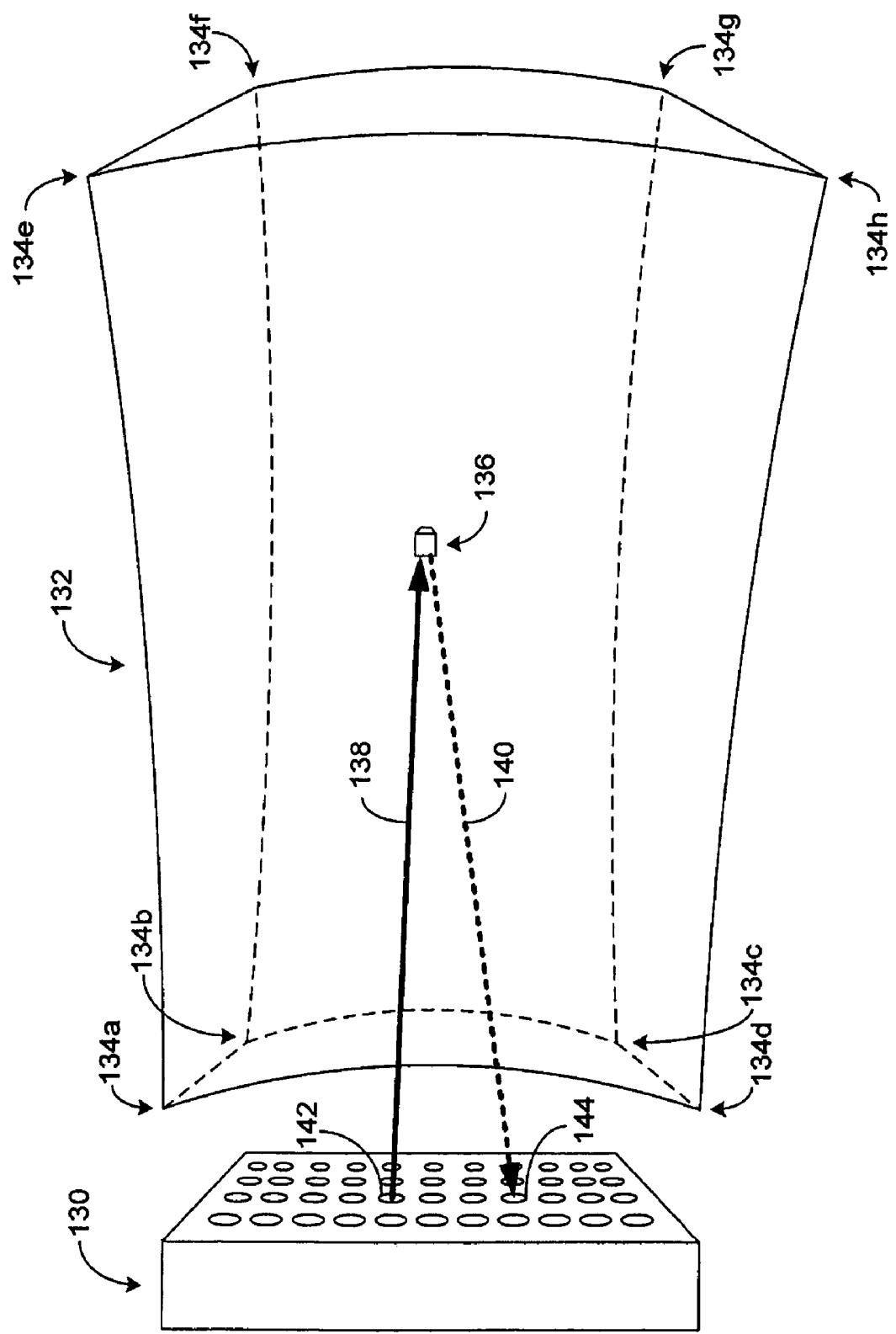


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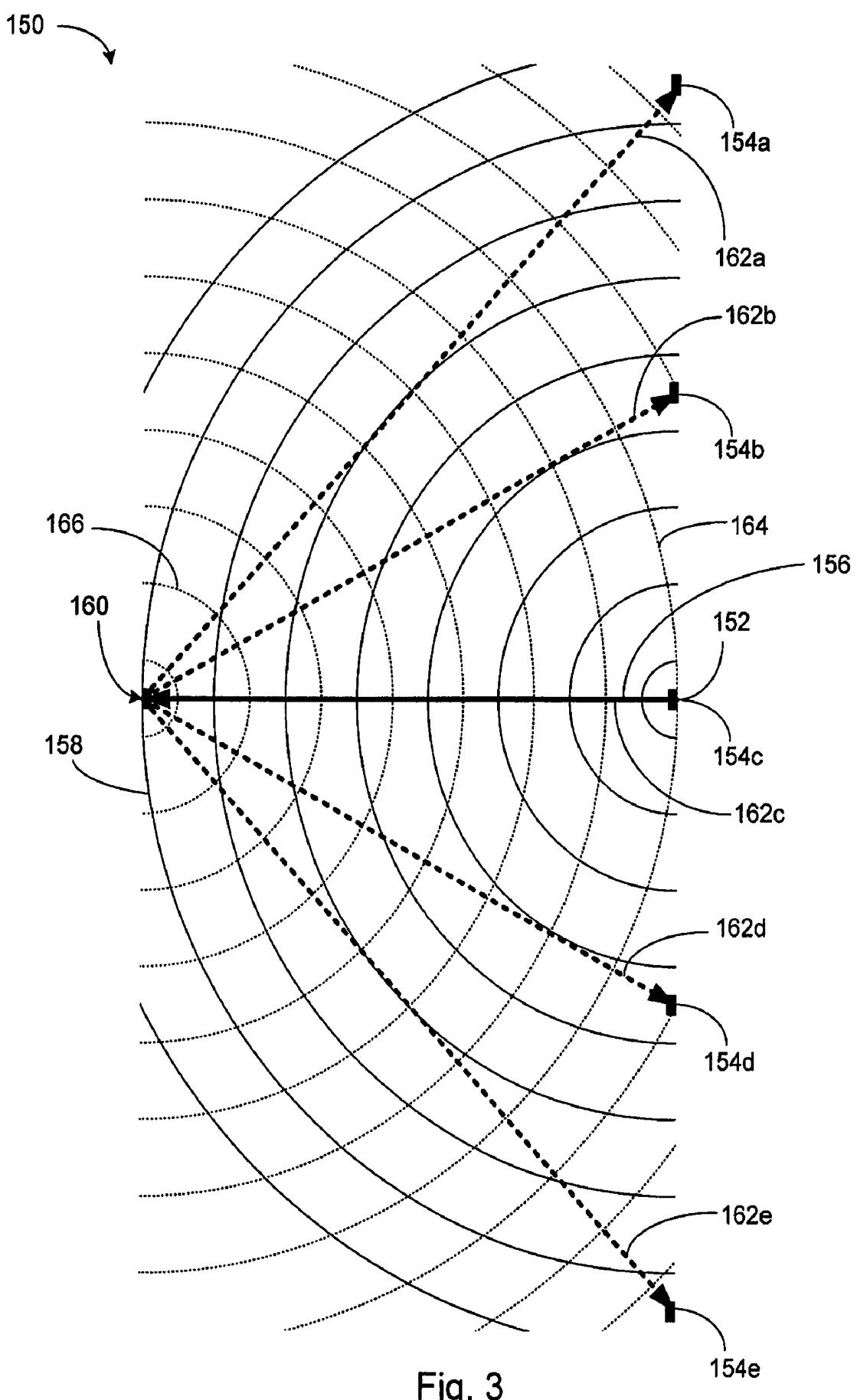
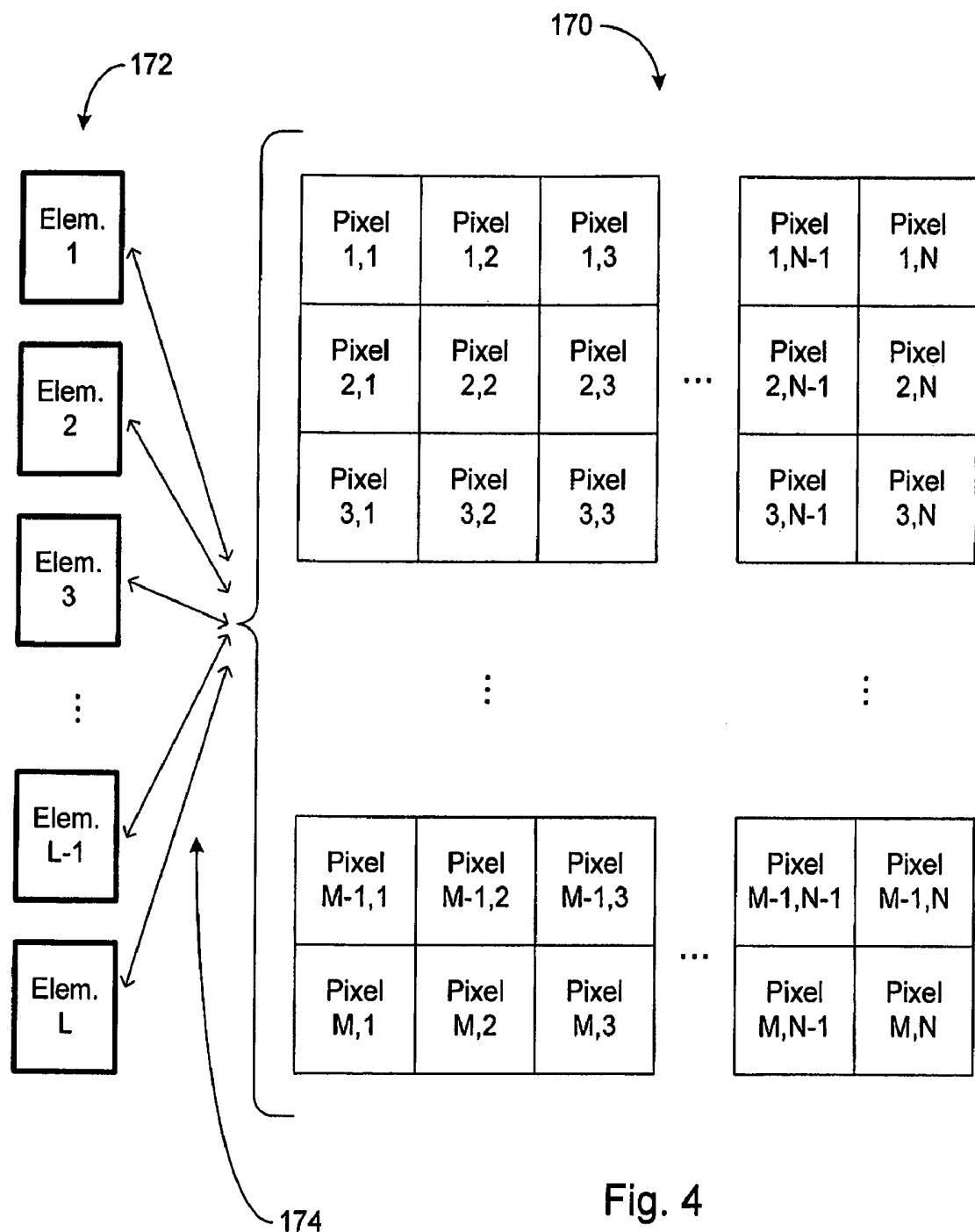


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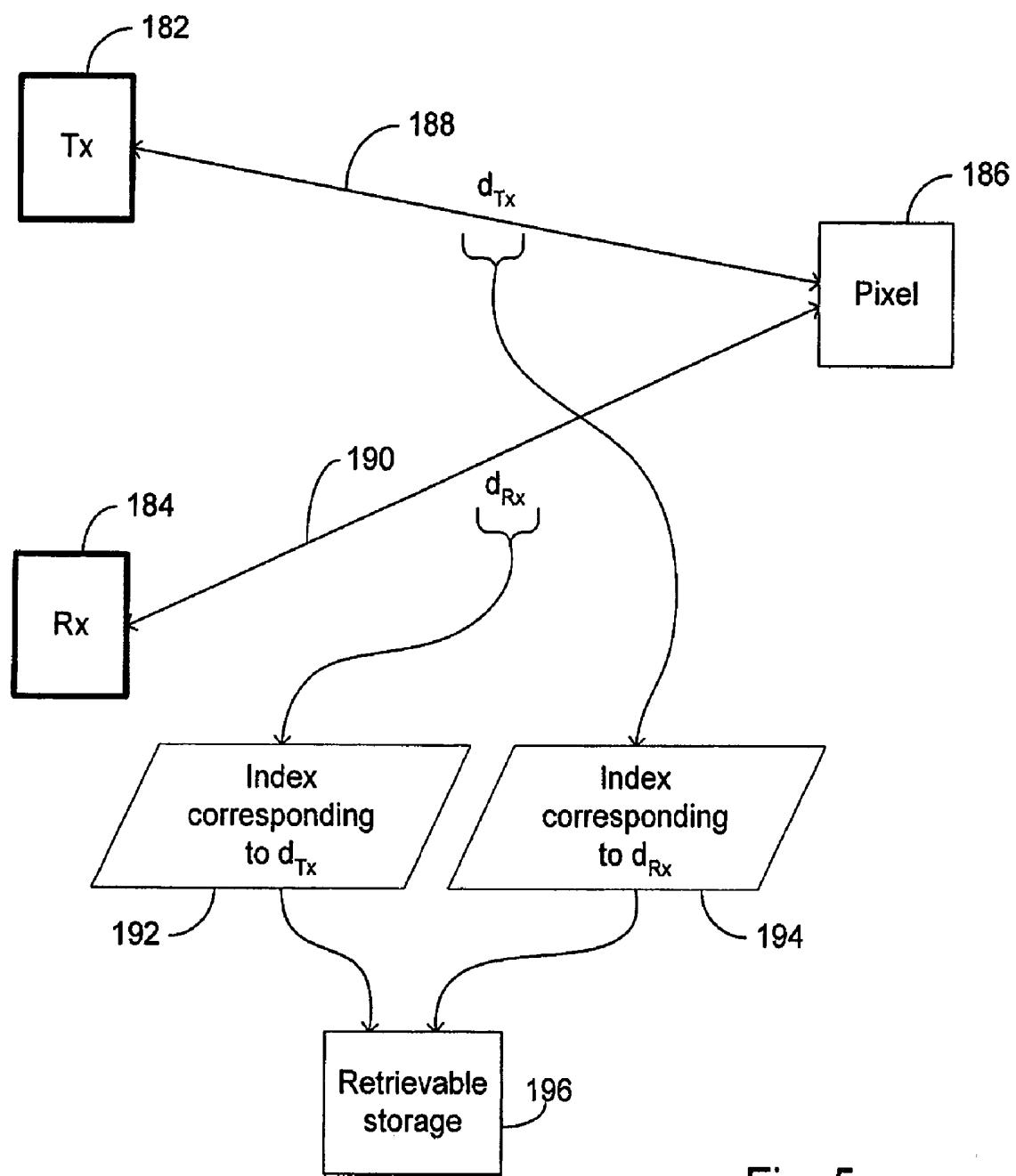


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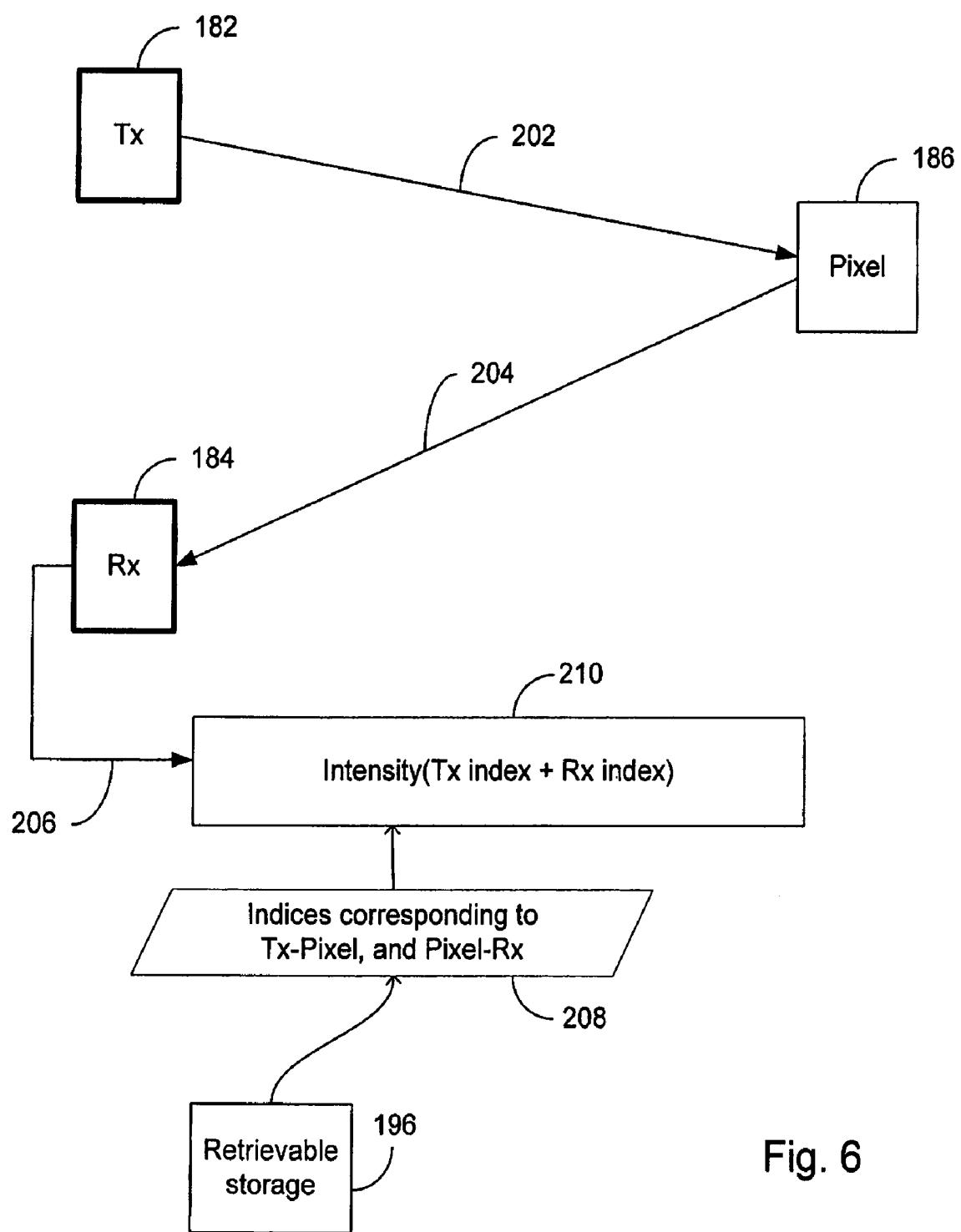


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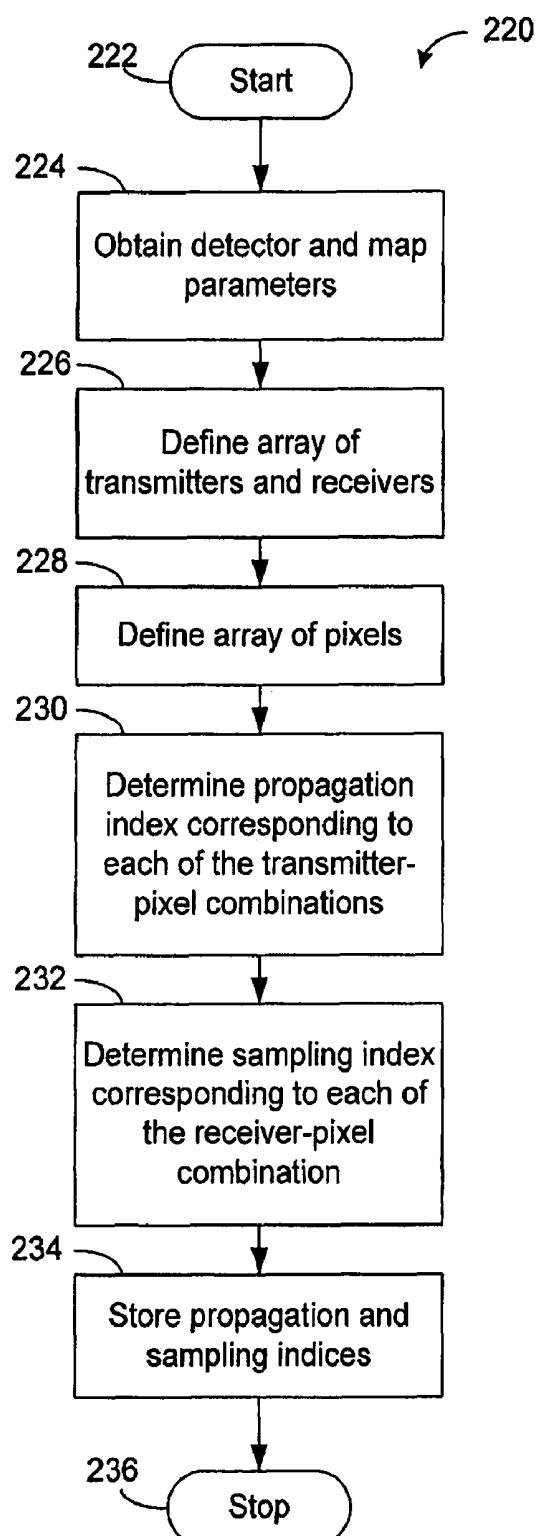


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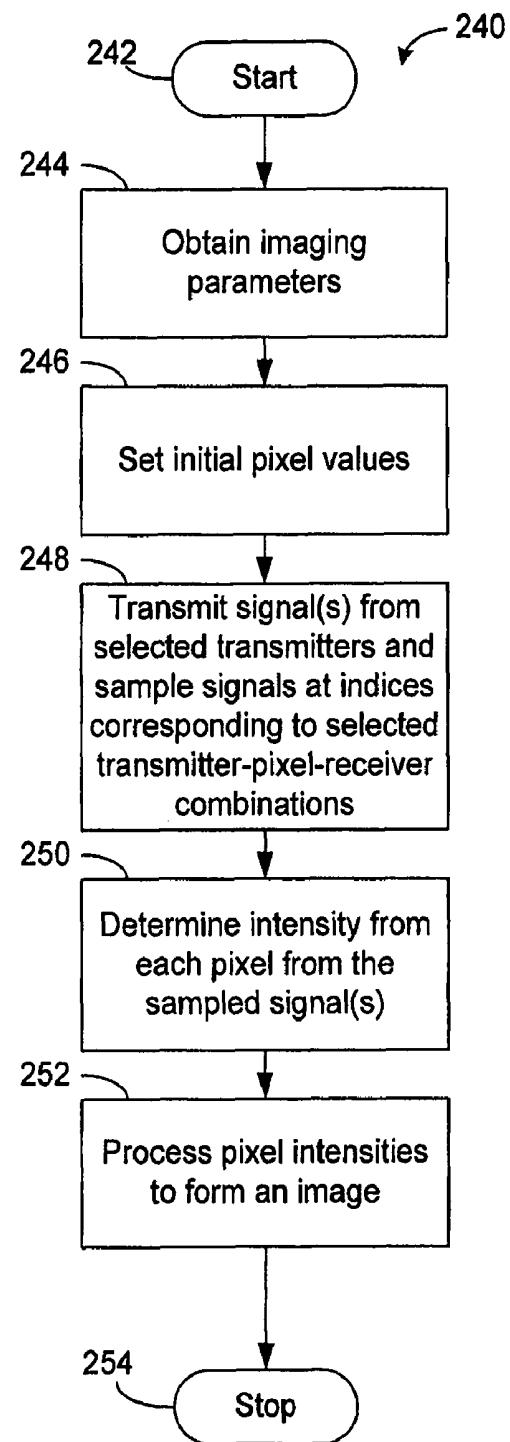


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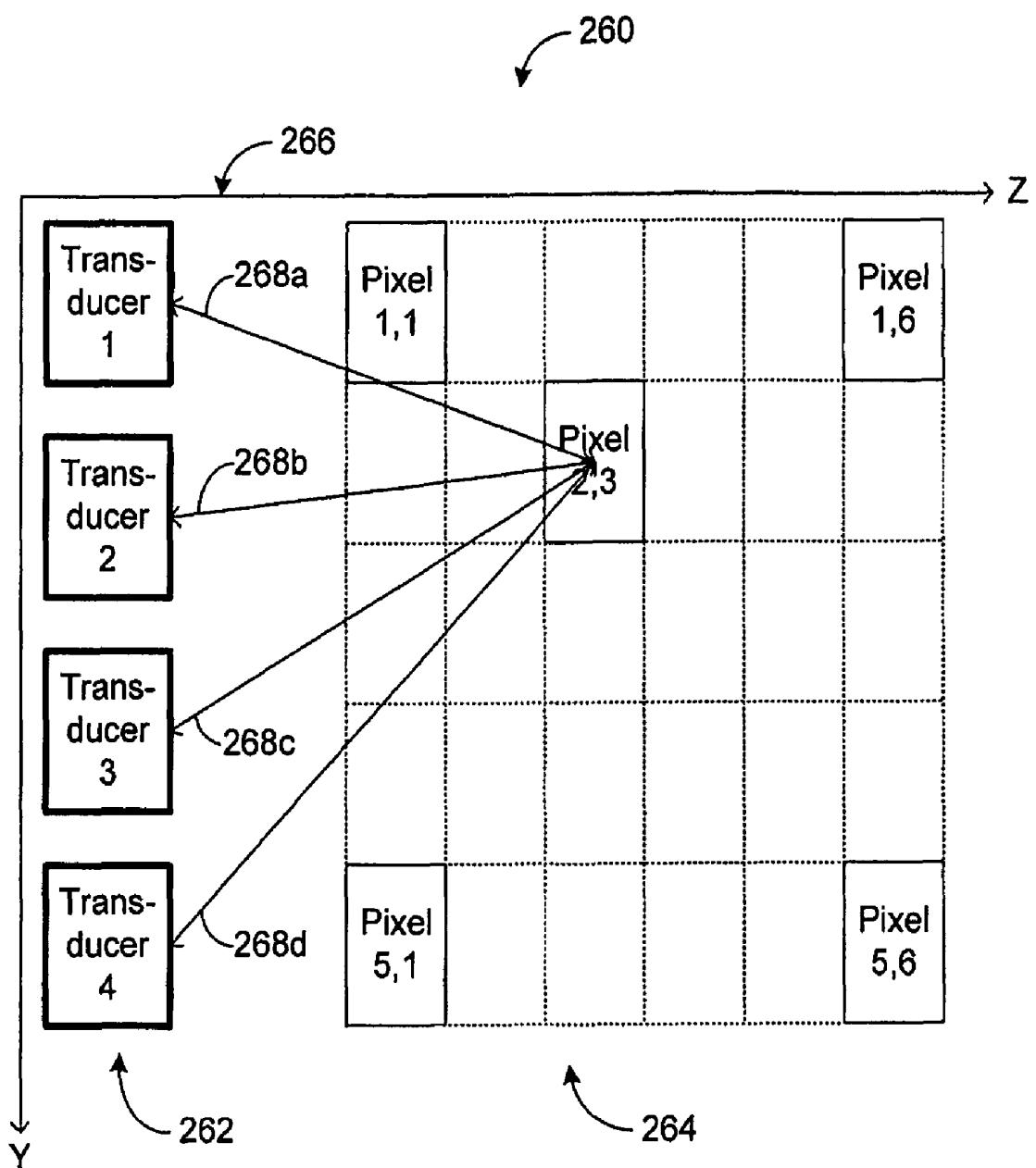


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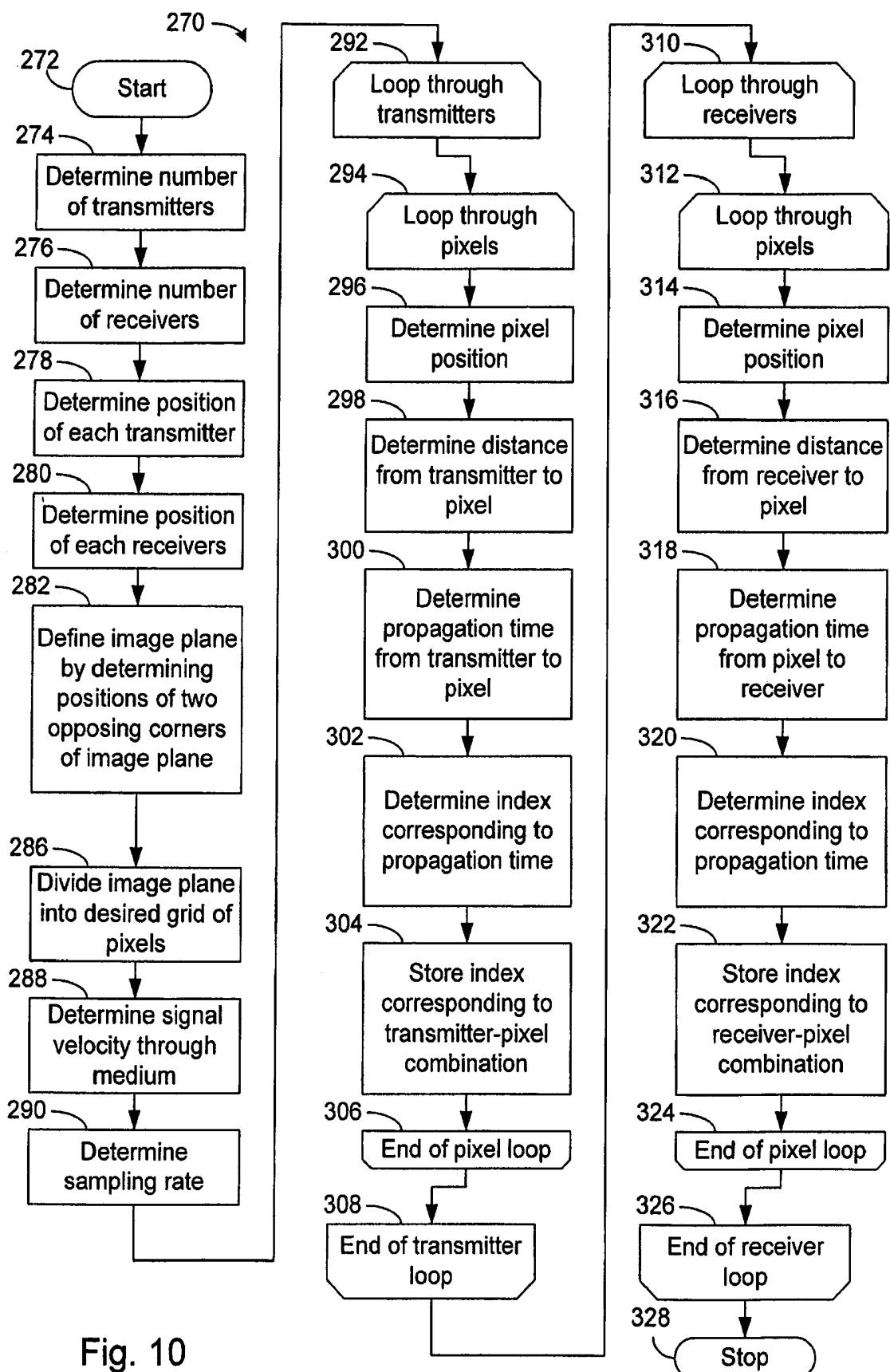


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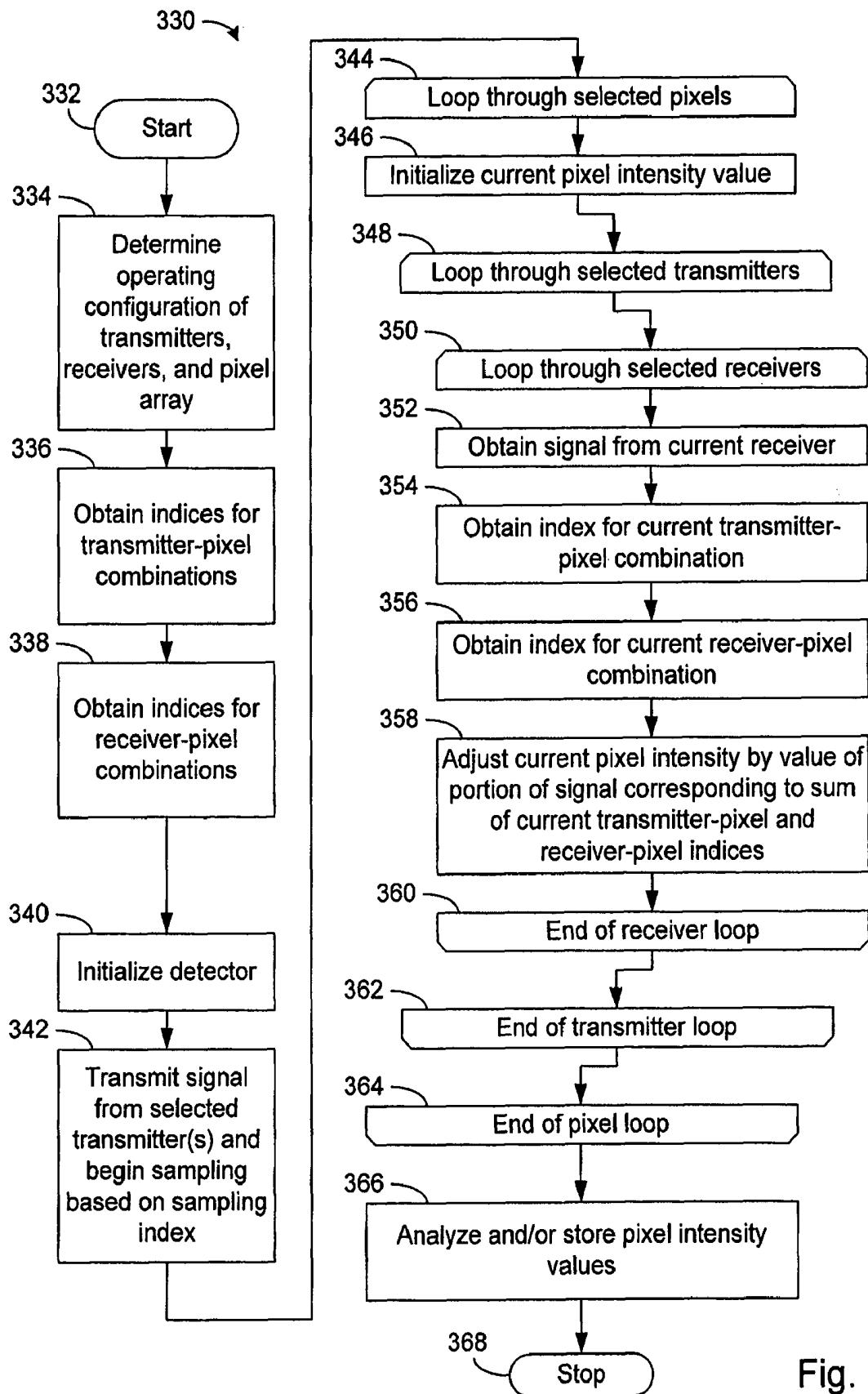


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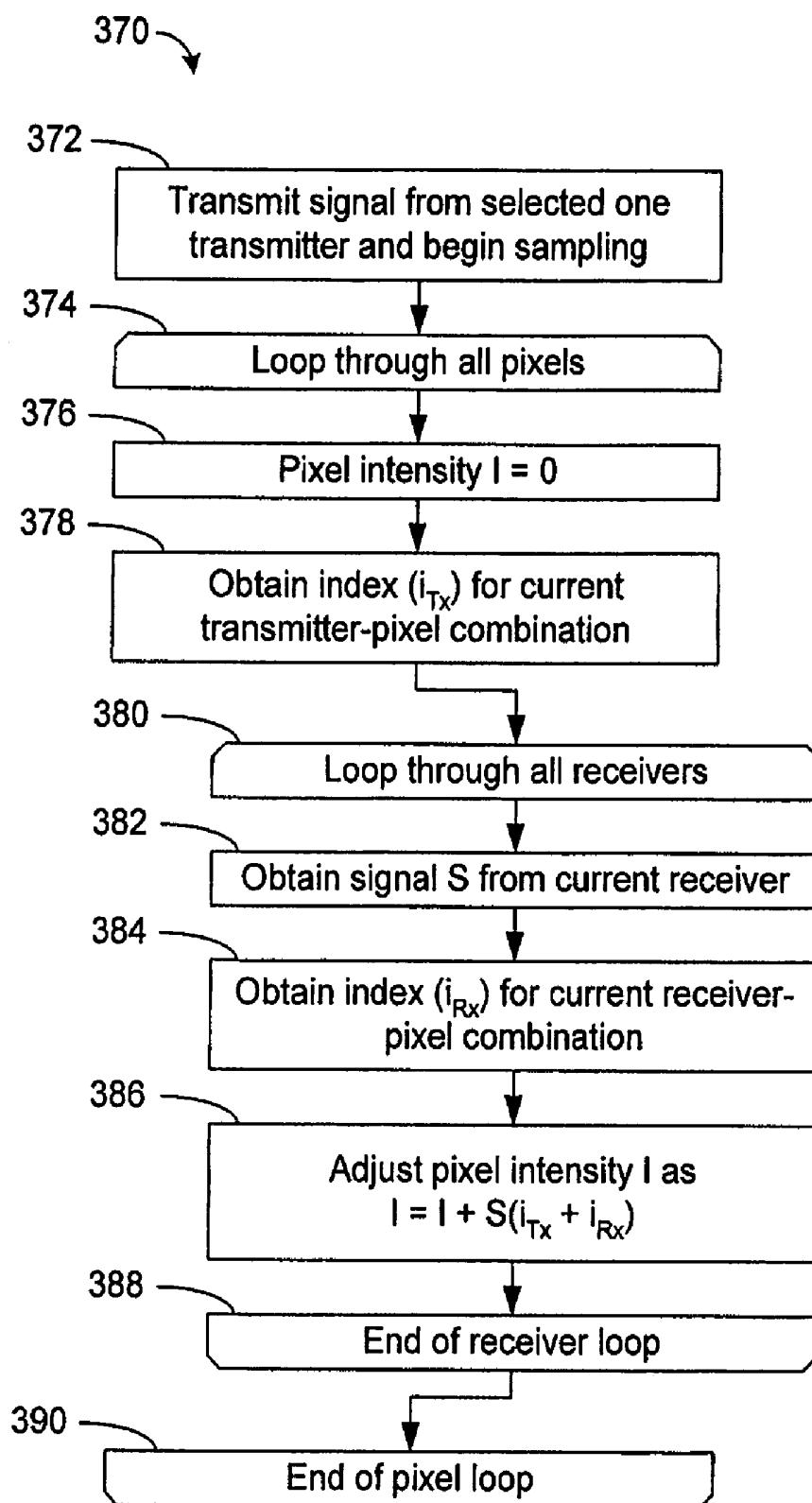


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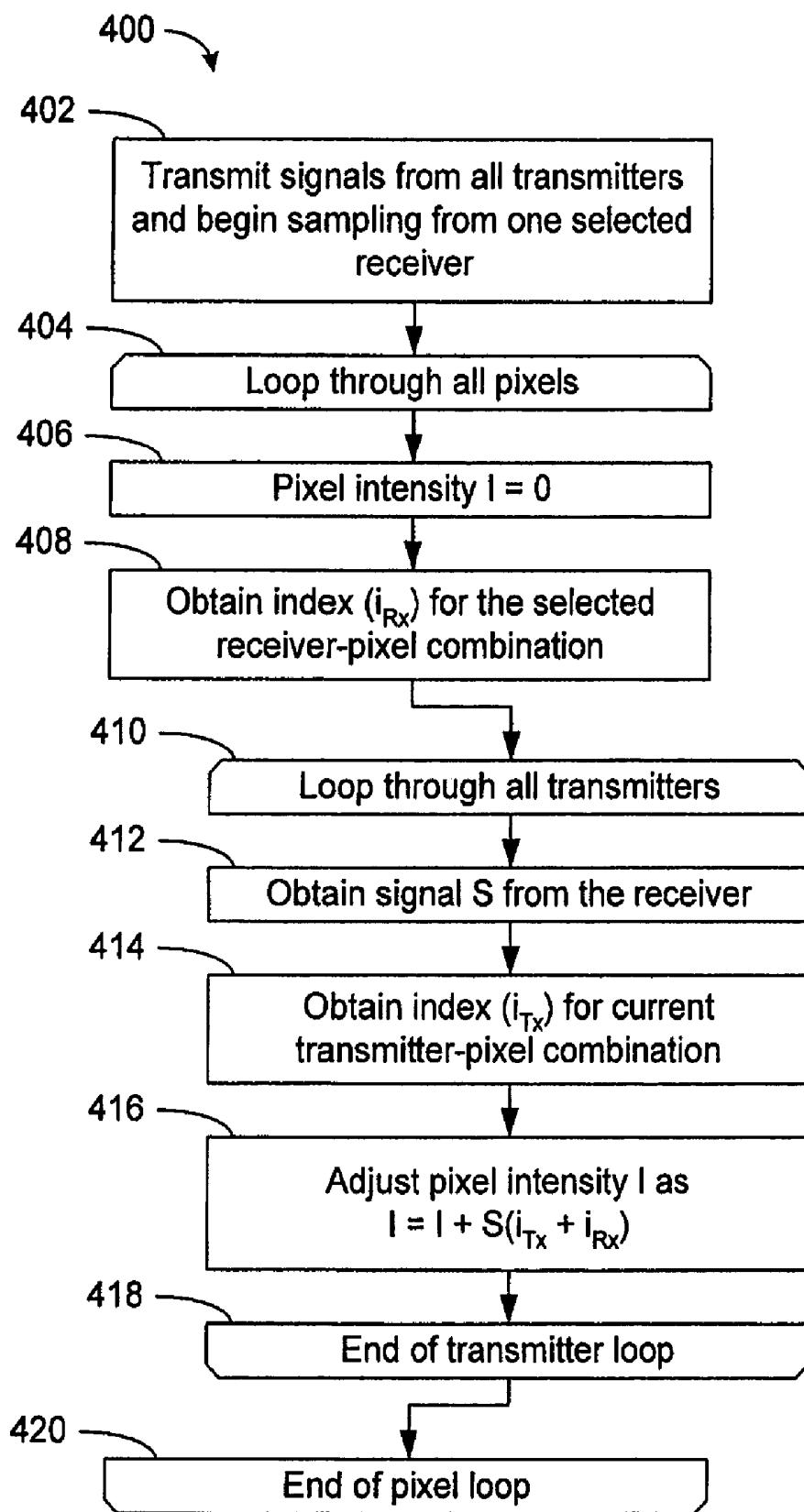


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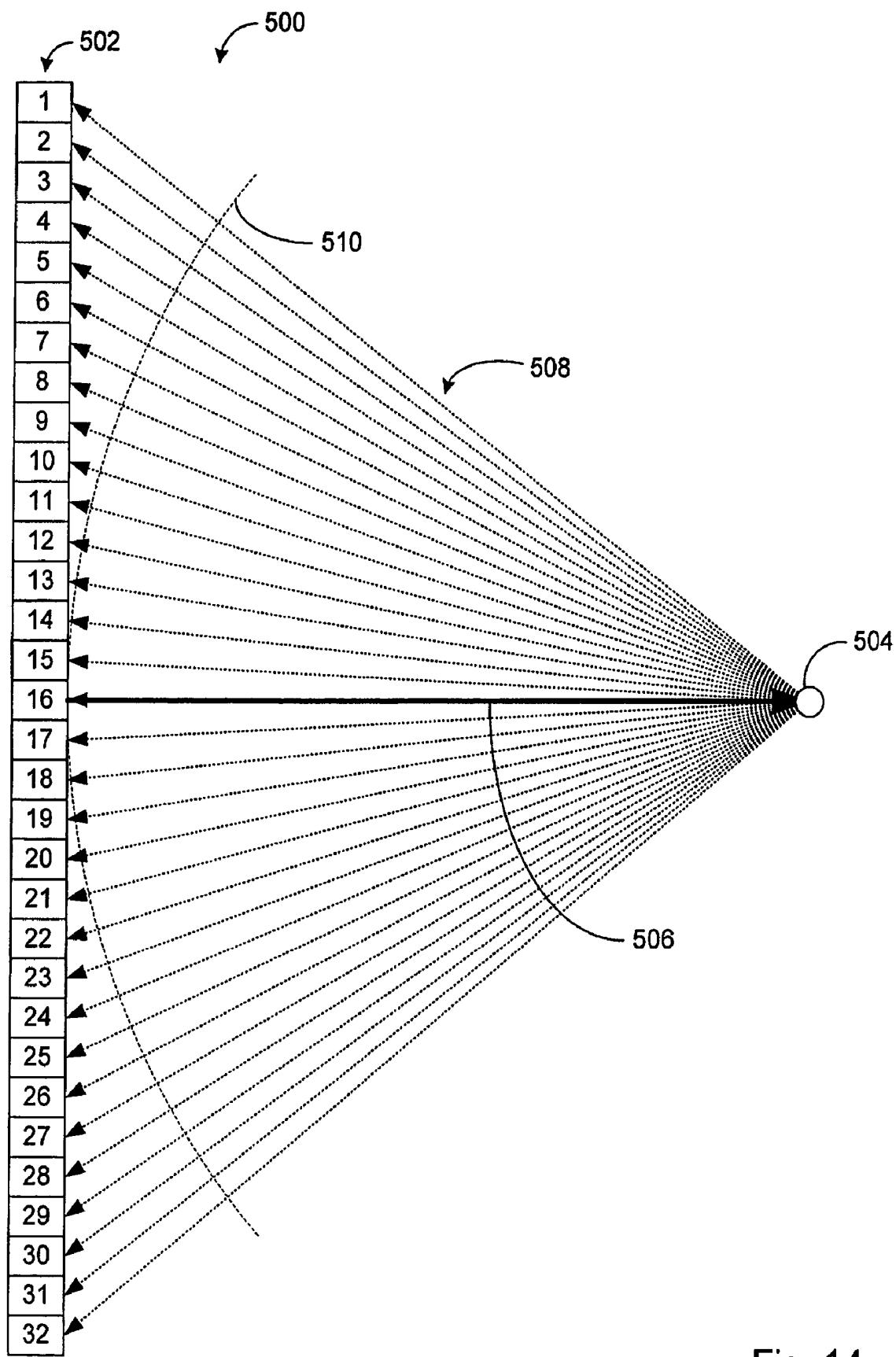


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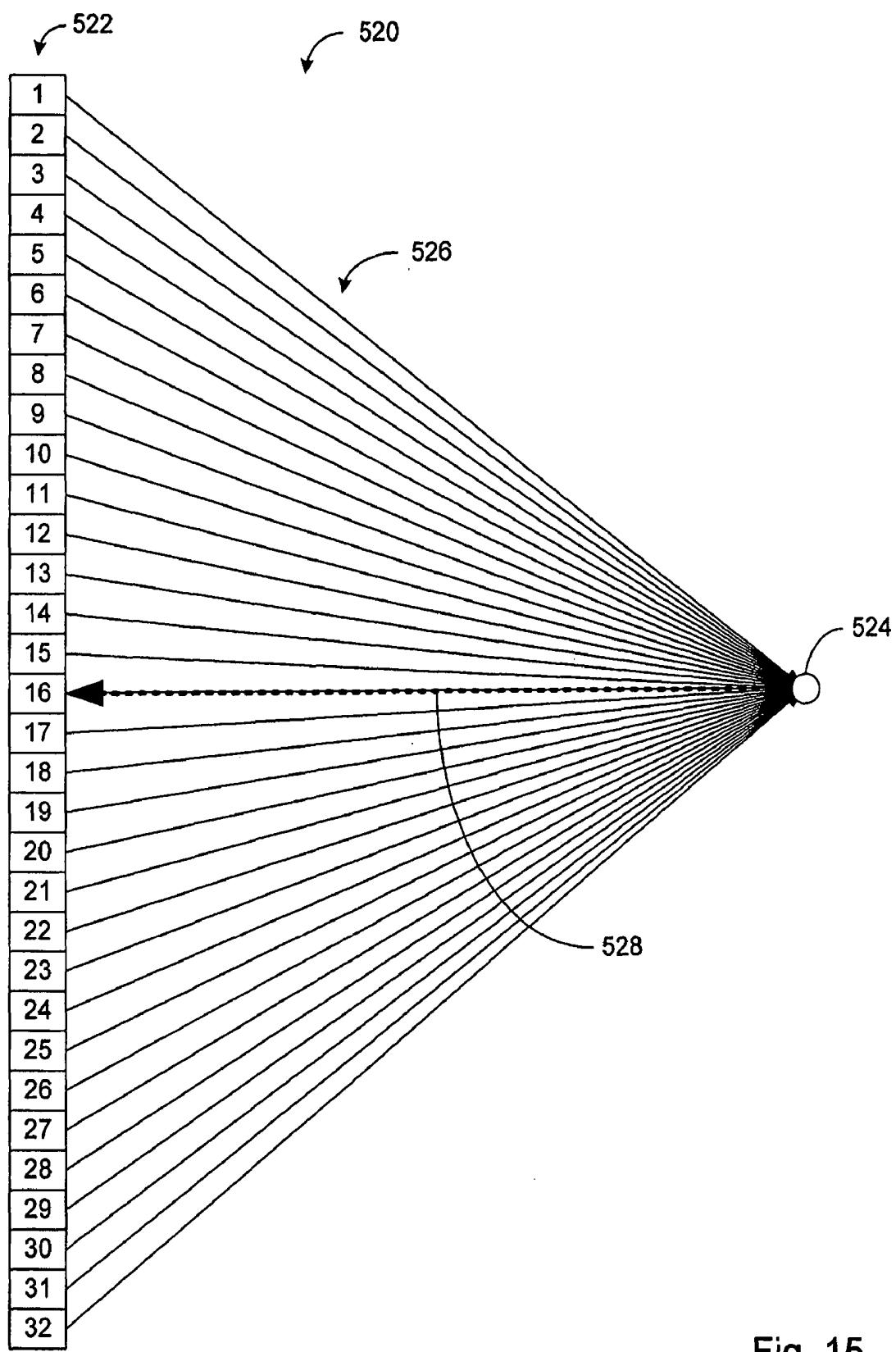


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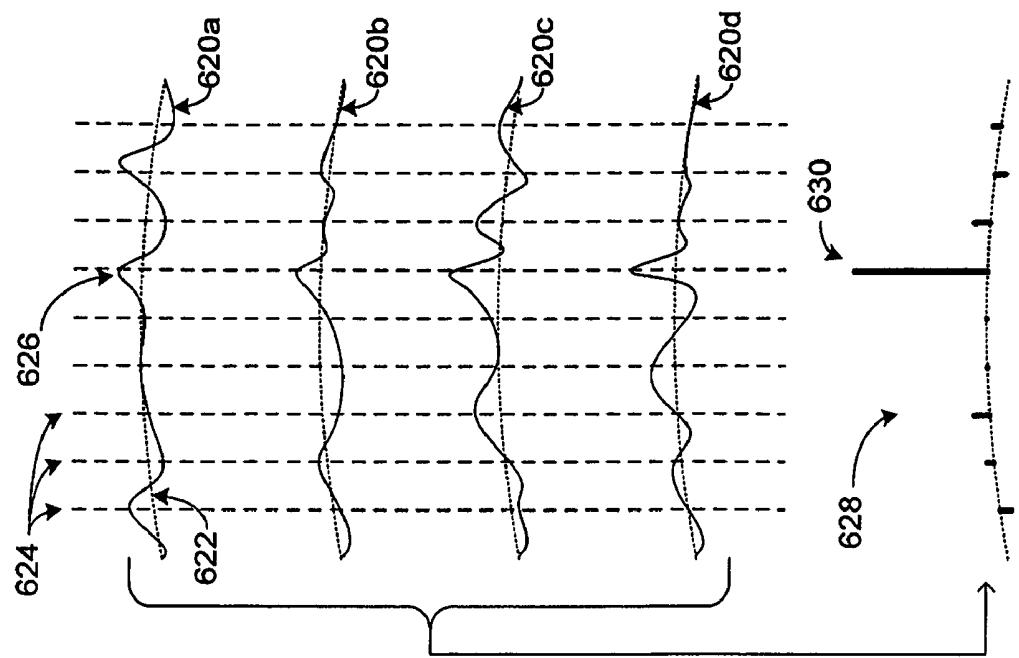


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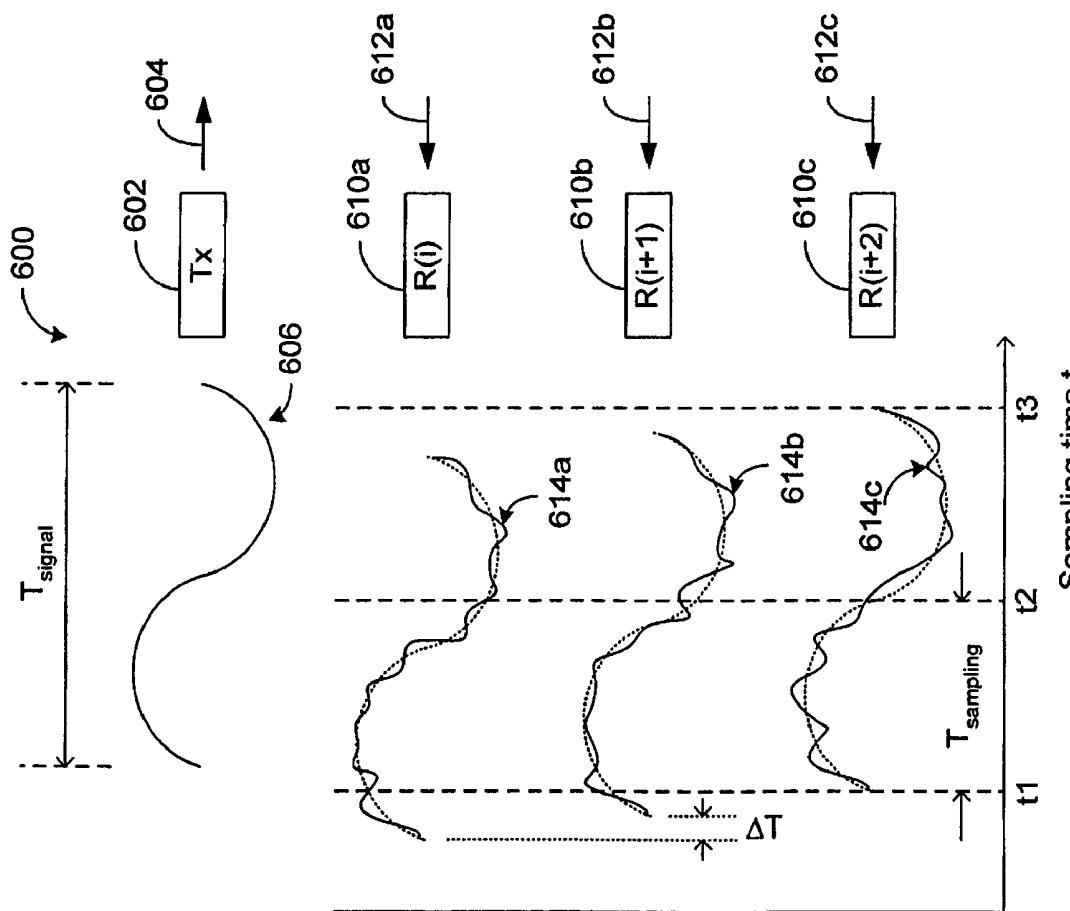


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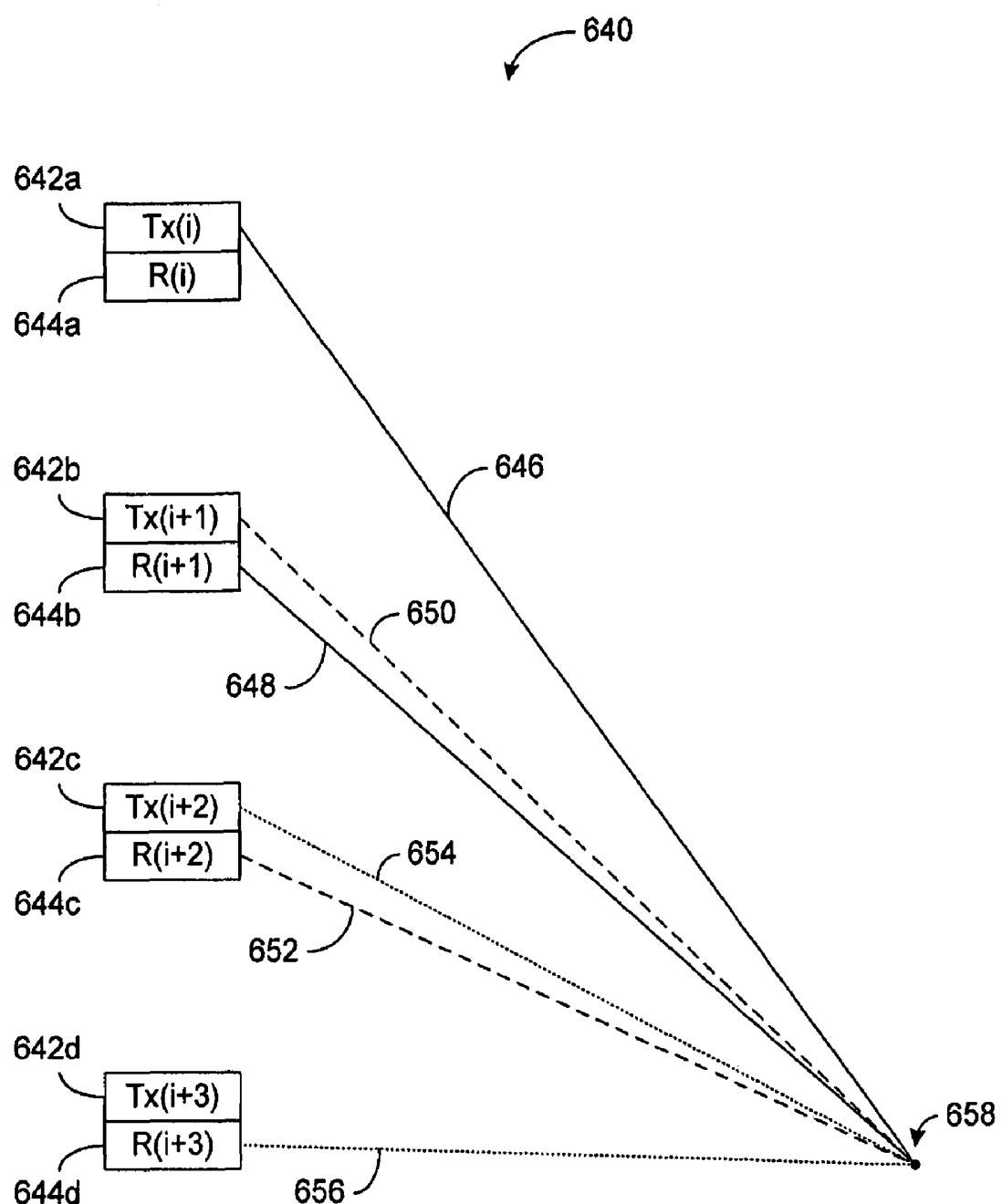


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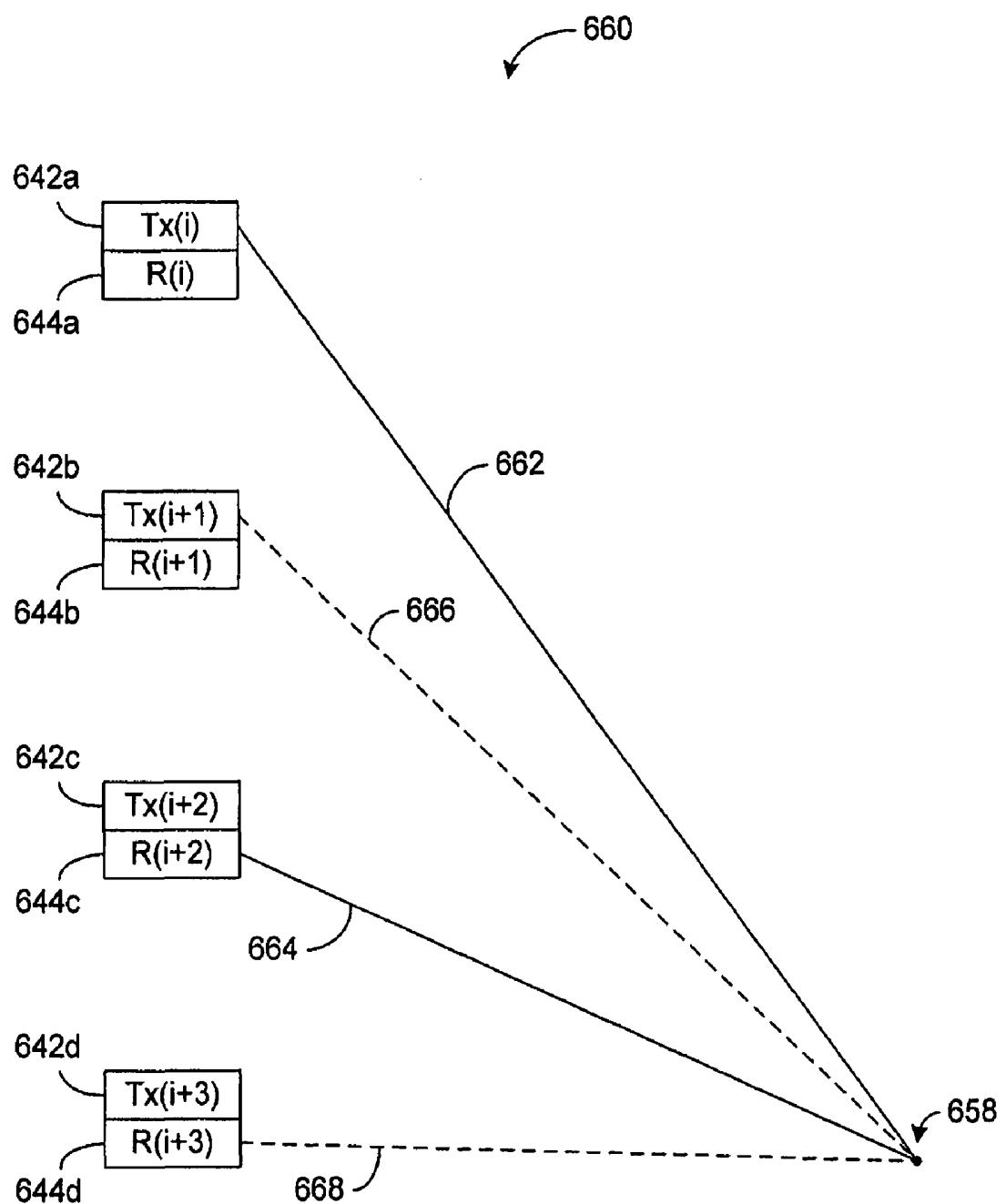


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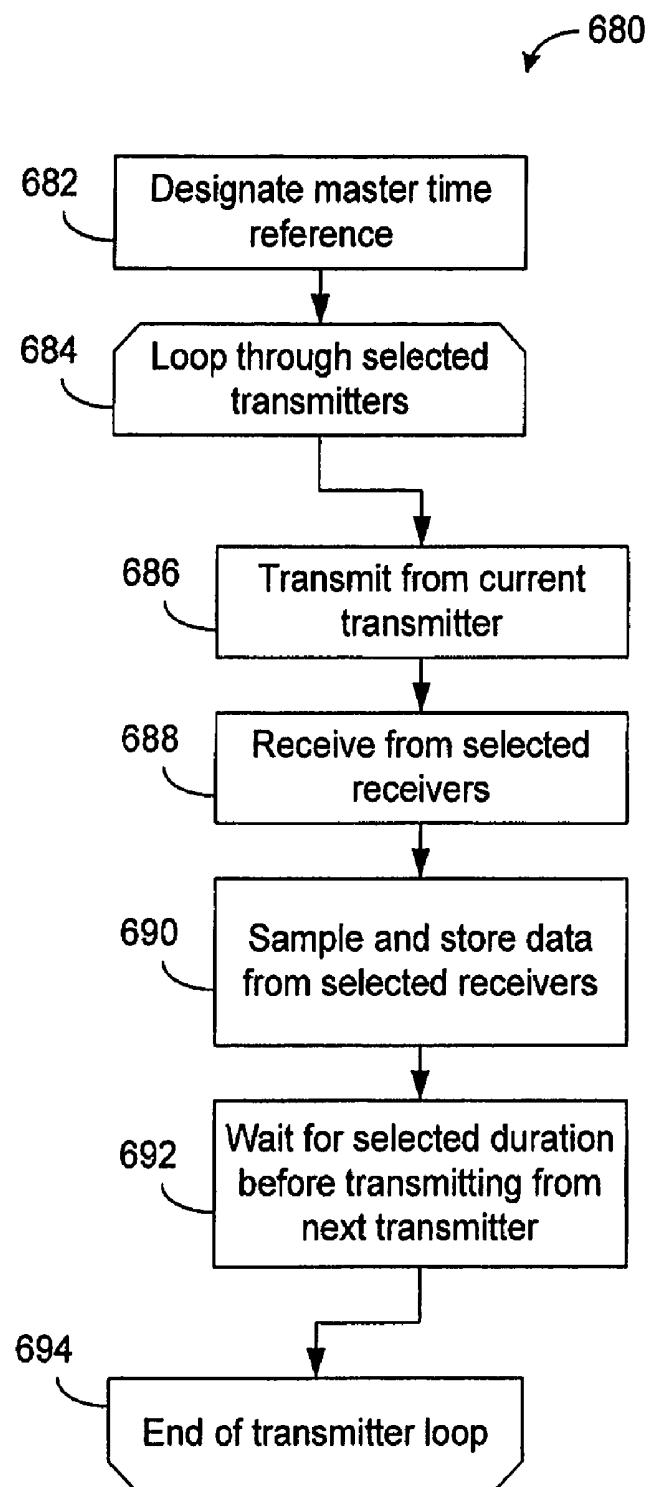


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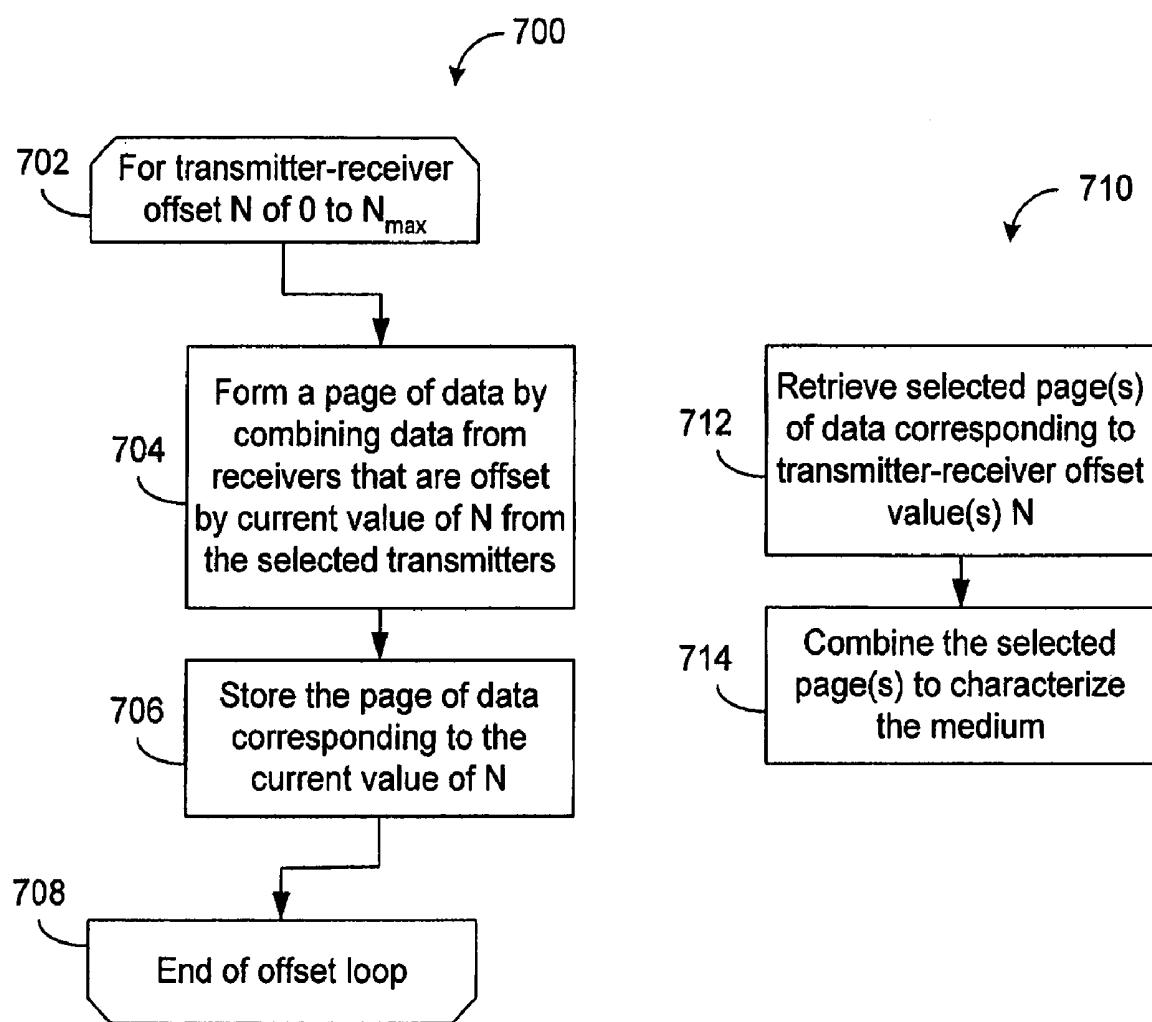


Fig. 20

Fig. 21

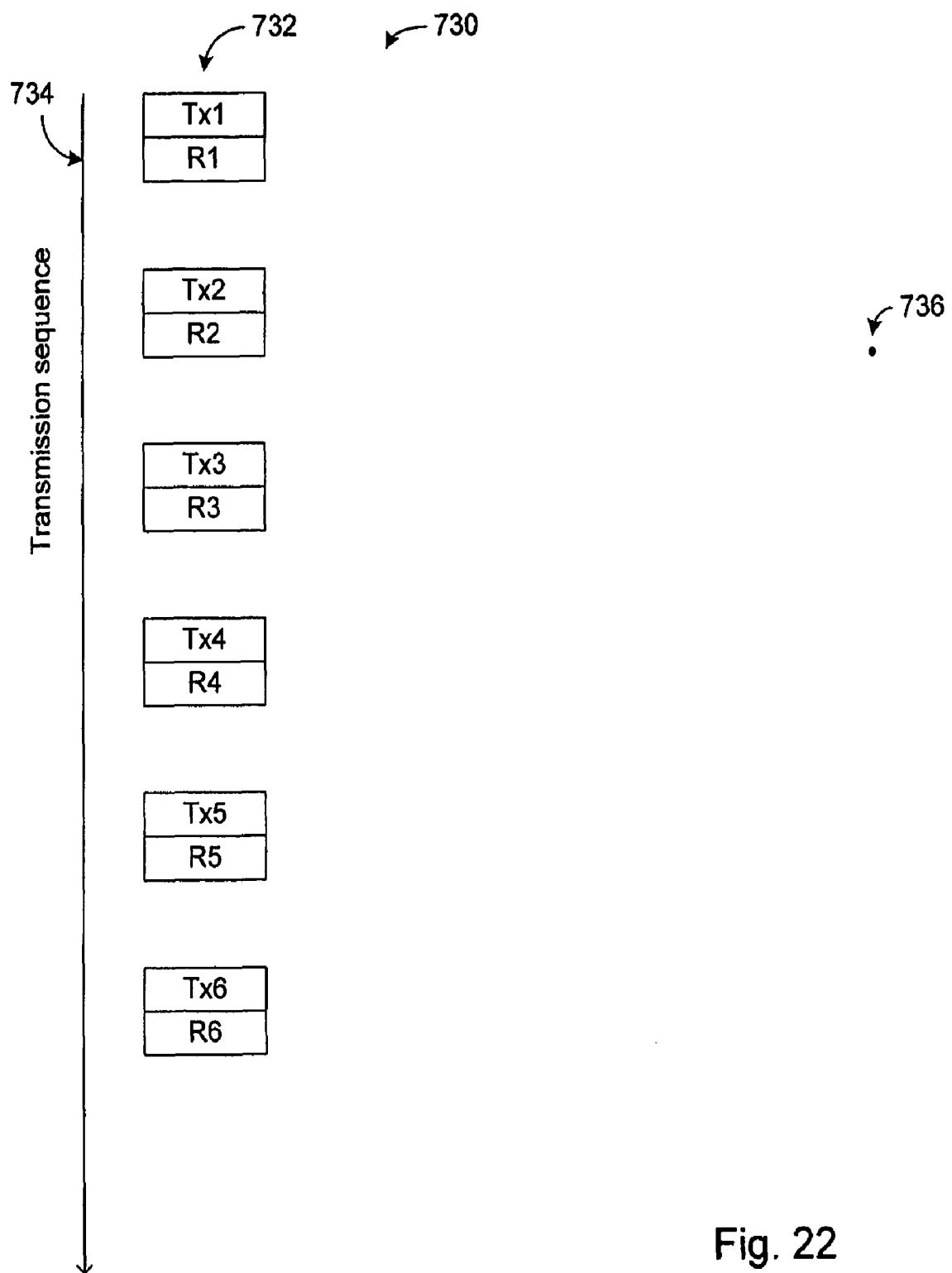


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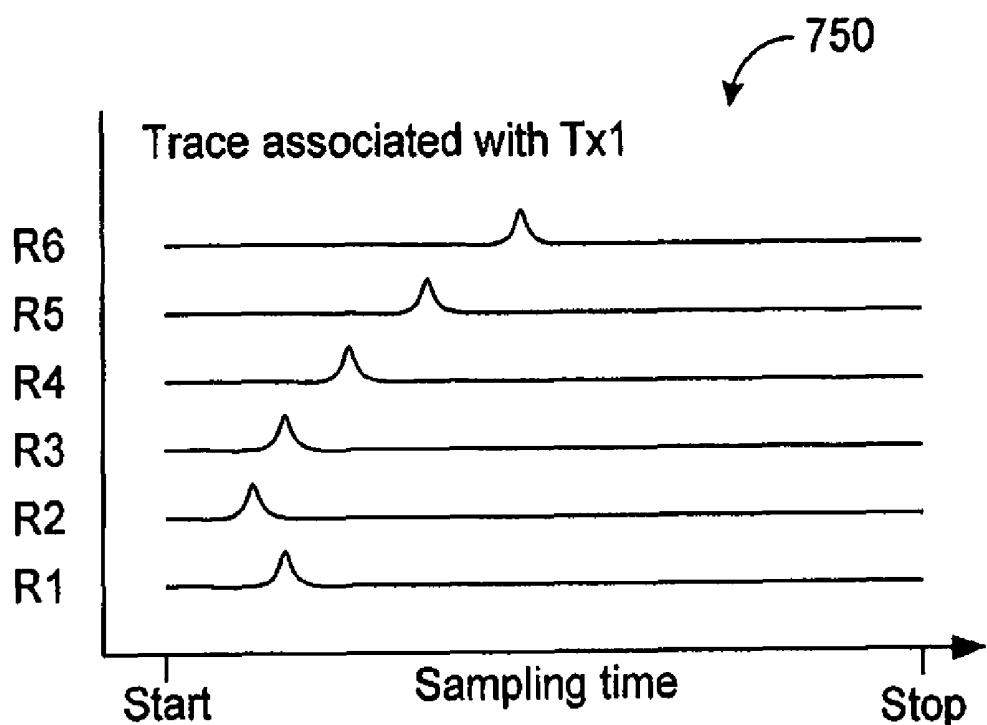


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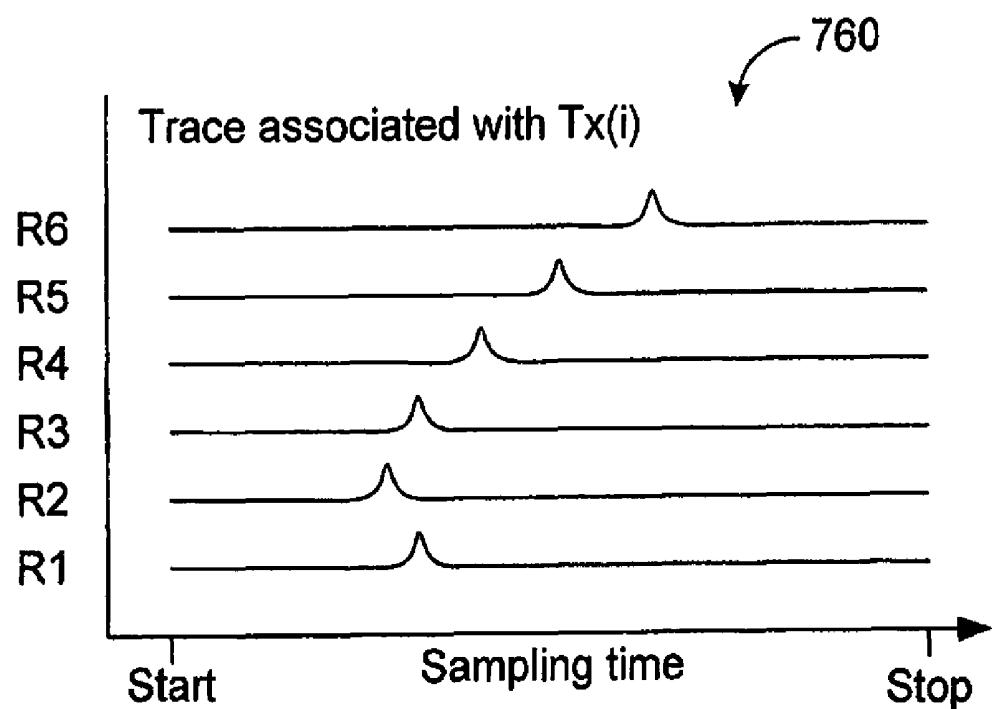
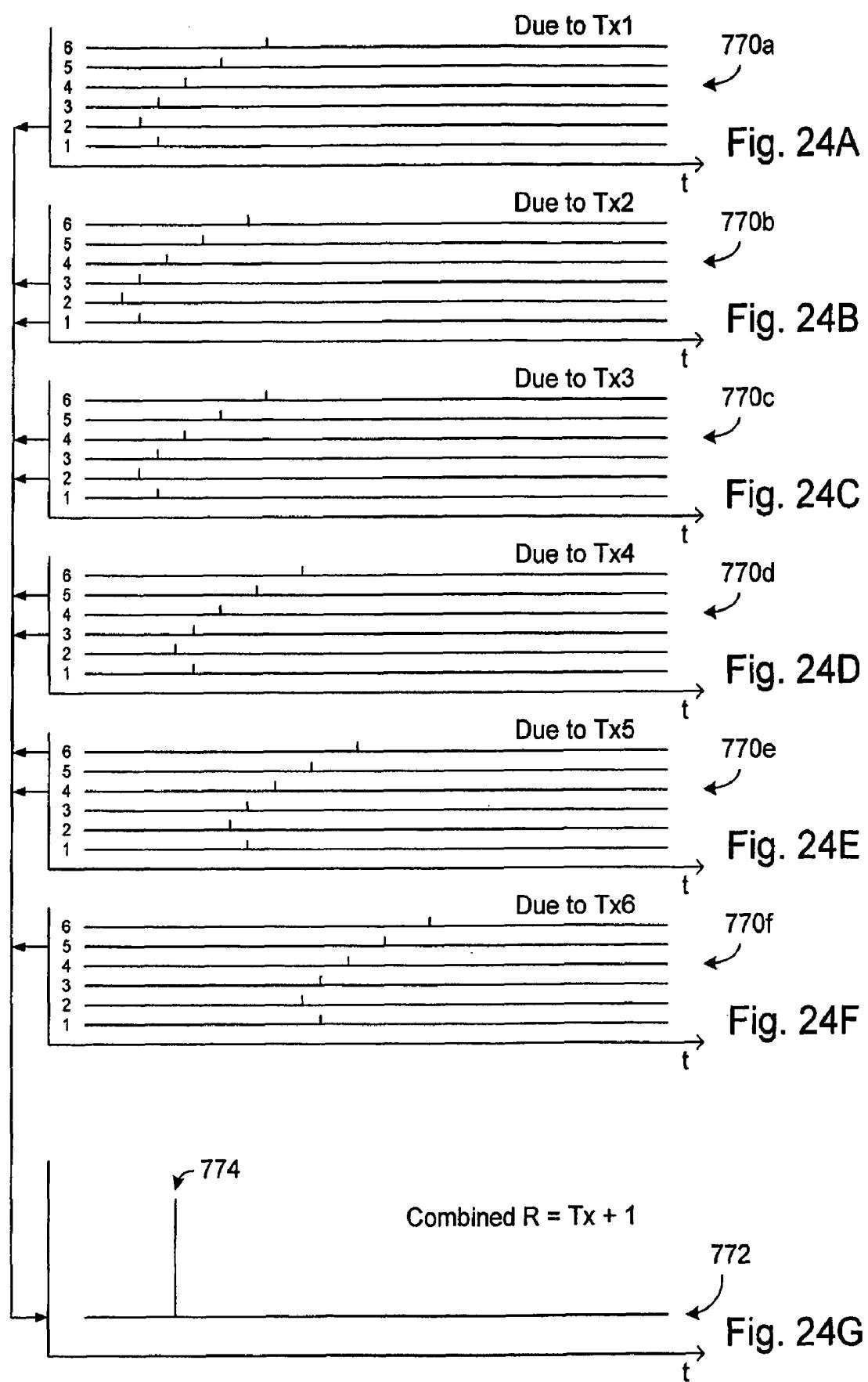
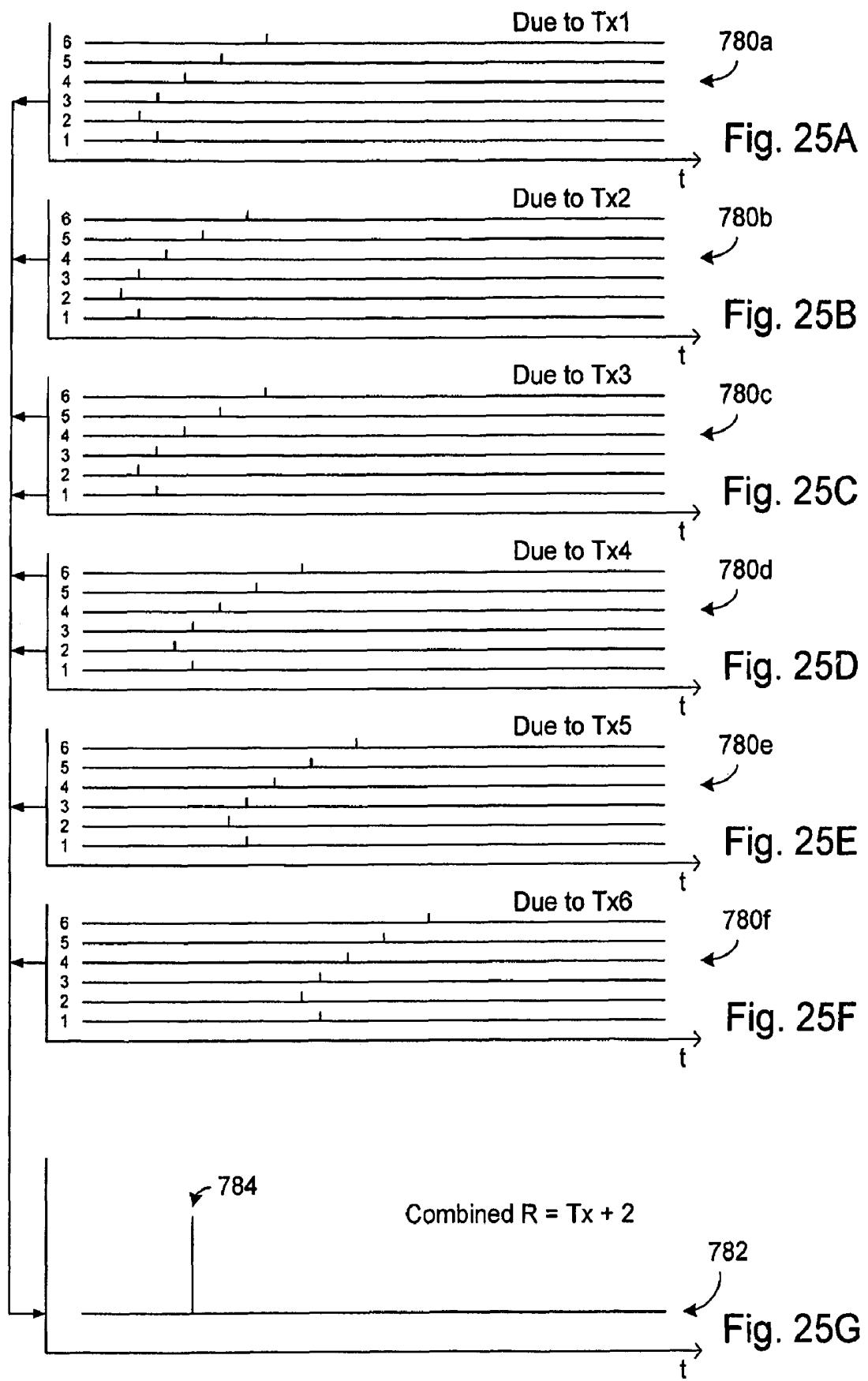


Fig. 23B





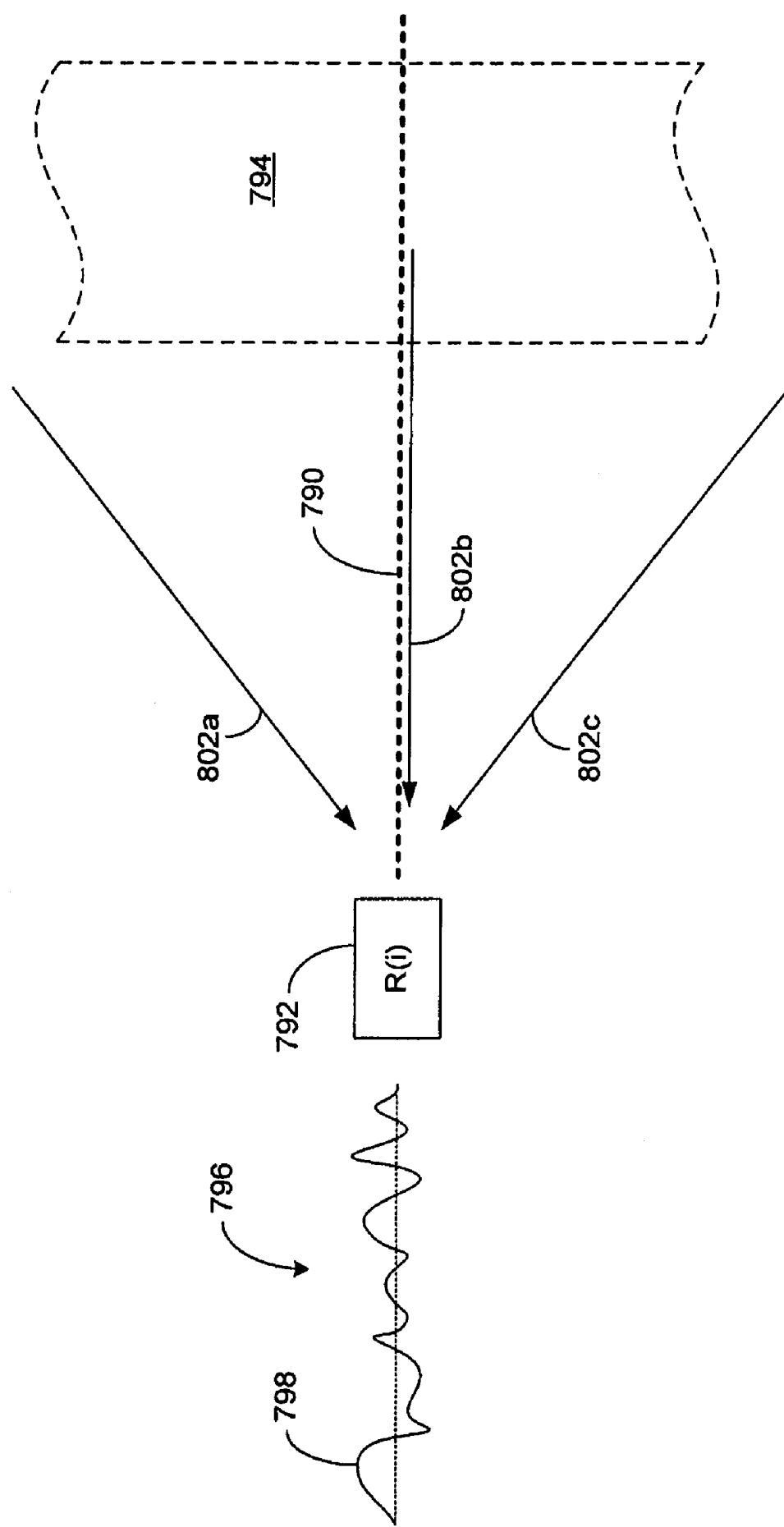


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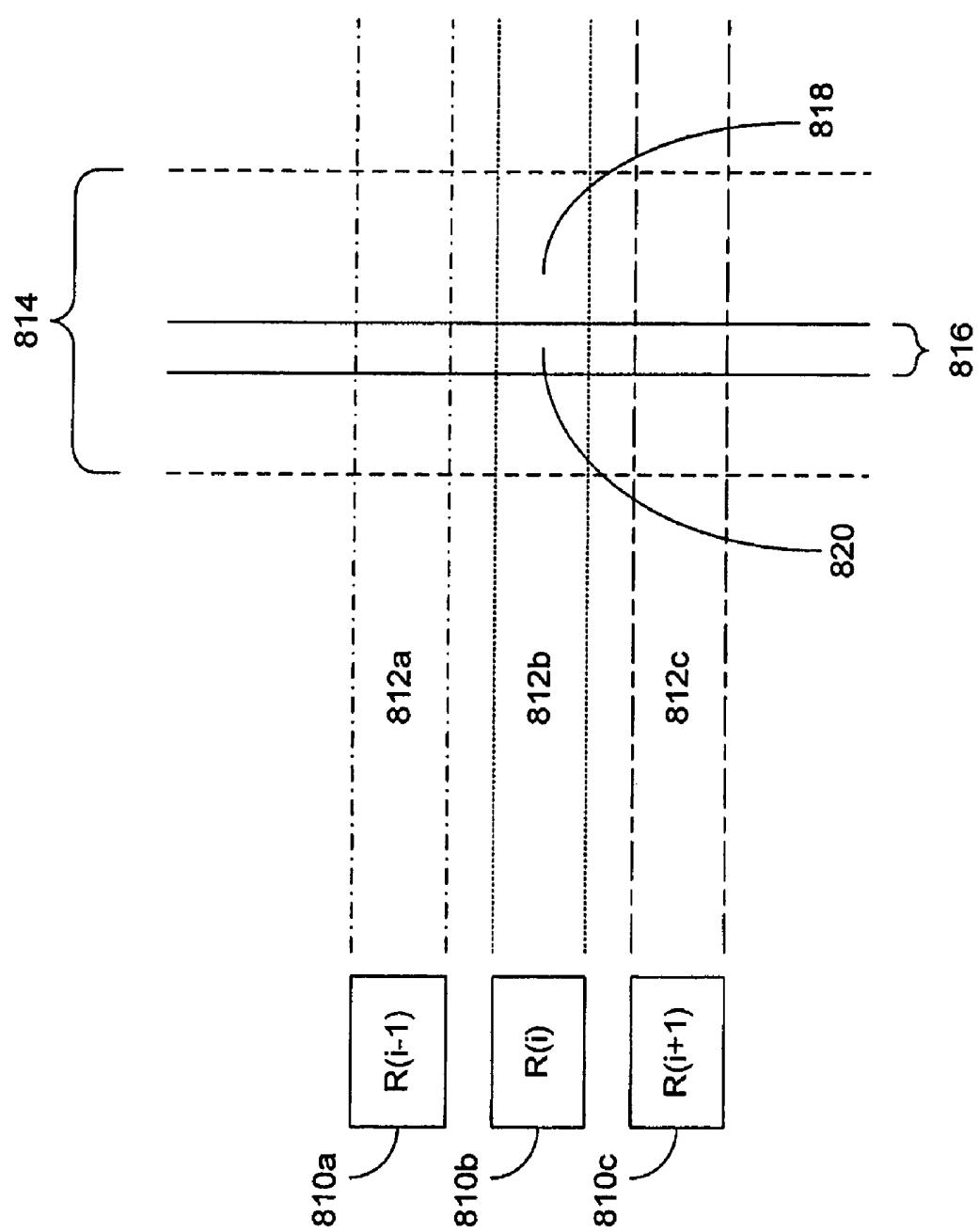
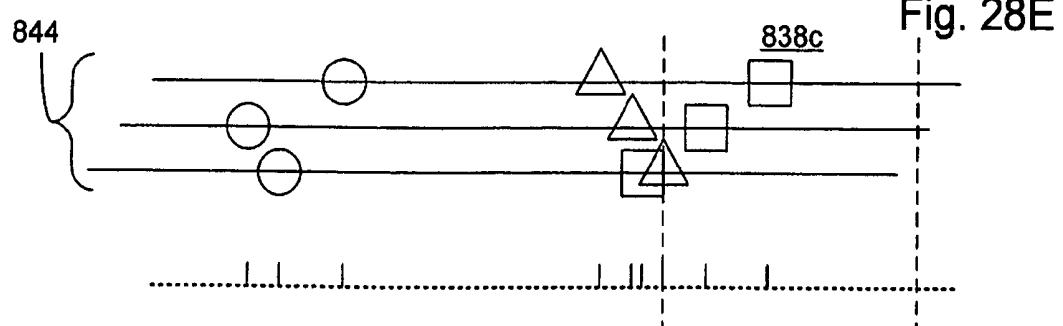
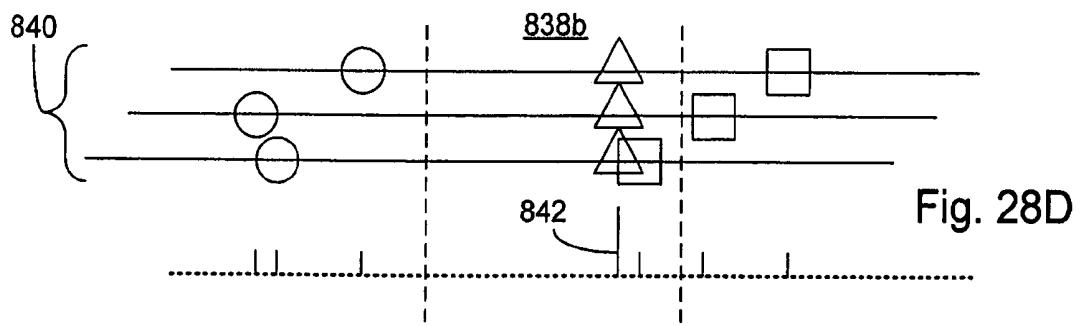
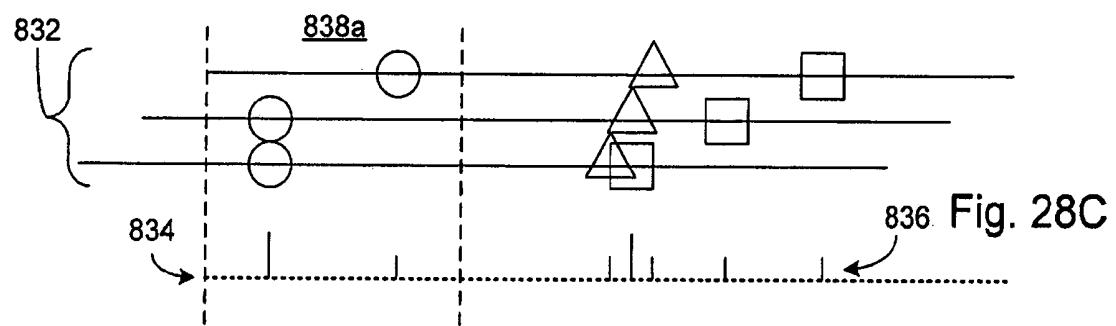
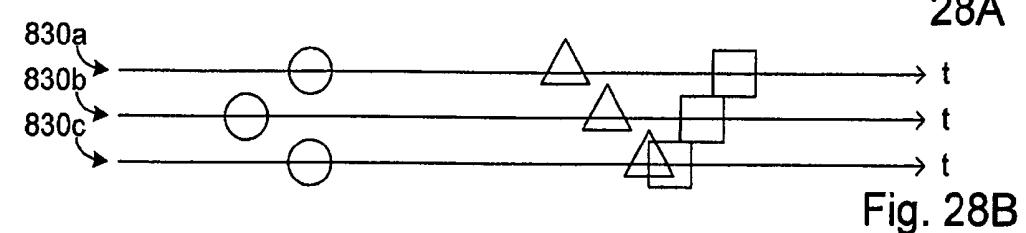
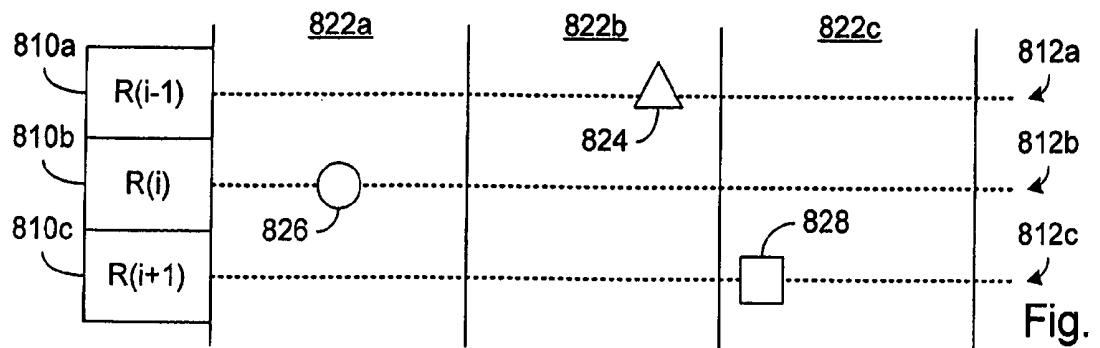


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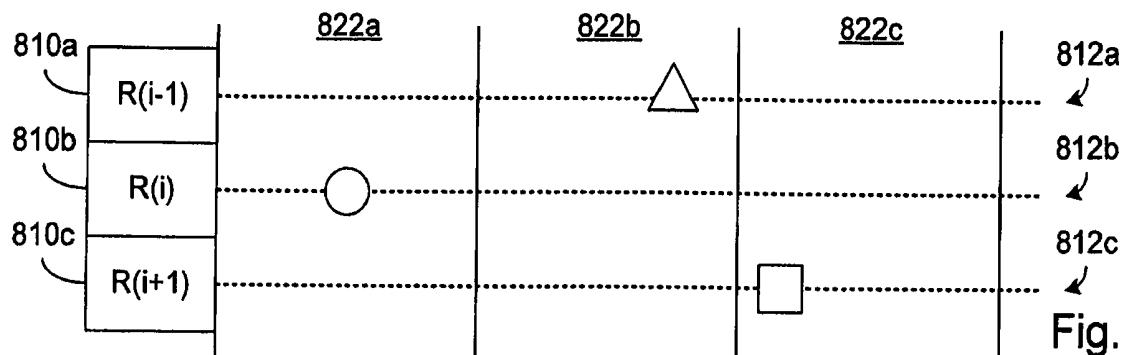


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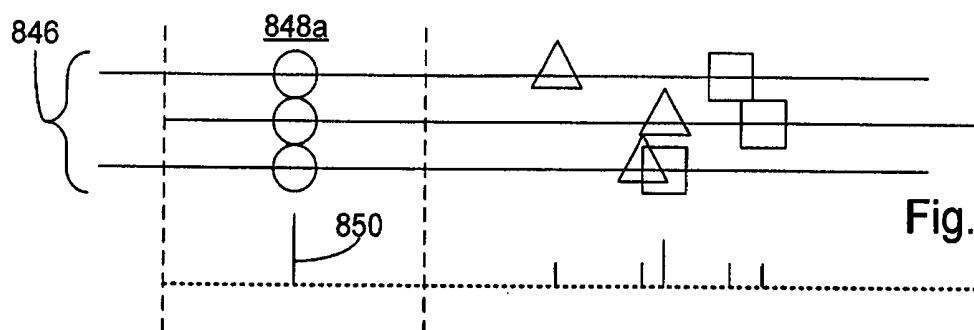


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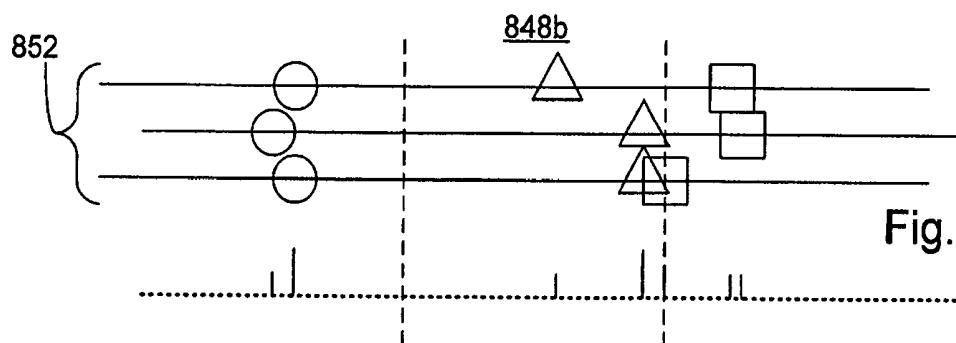


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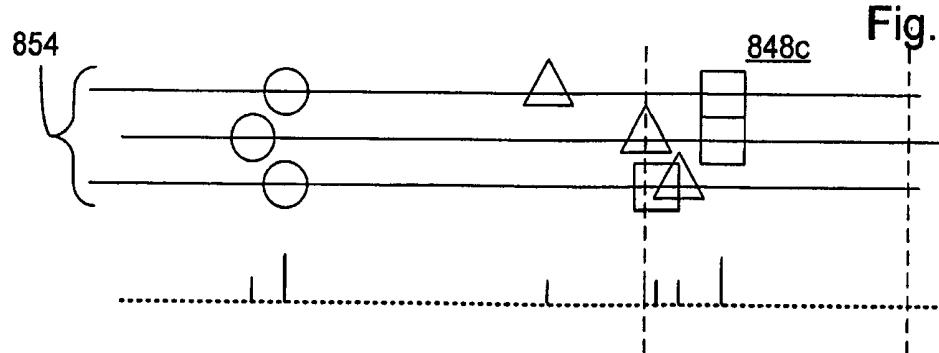
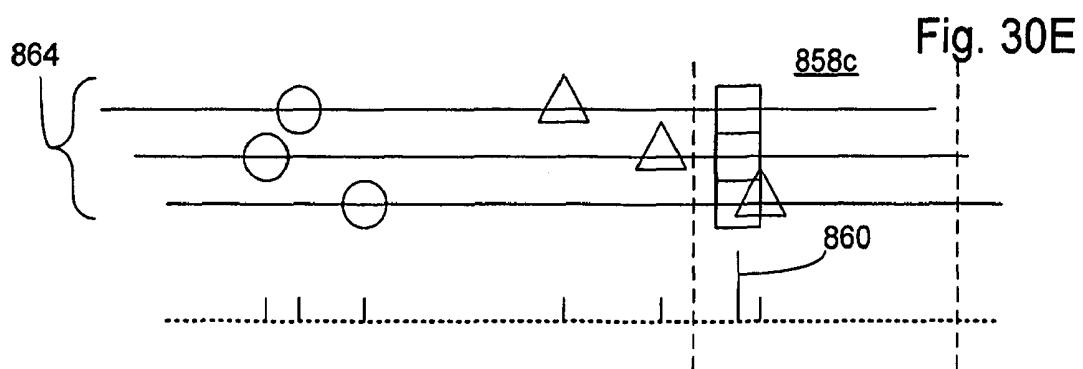
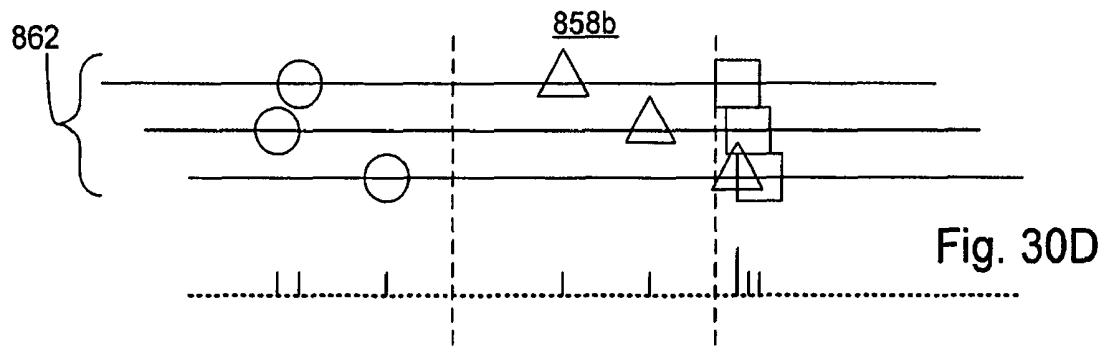
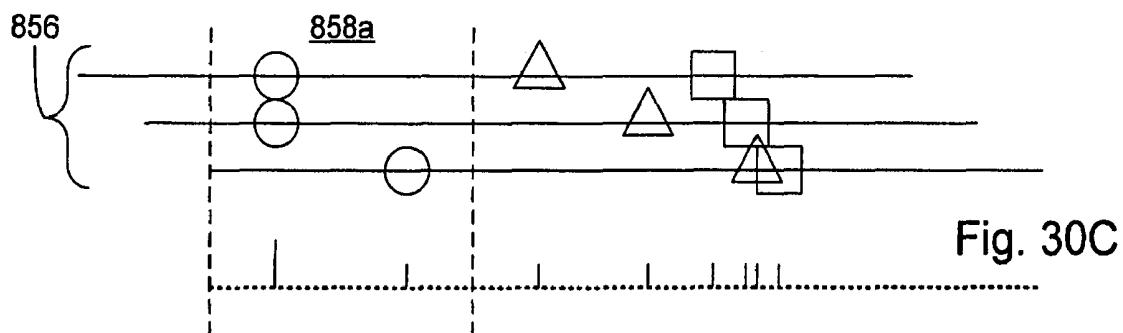
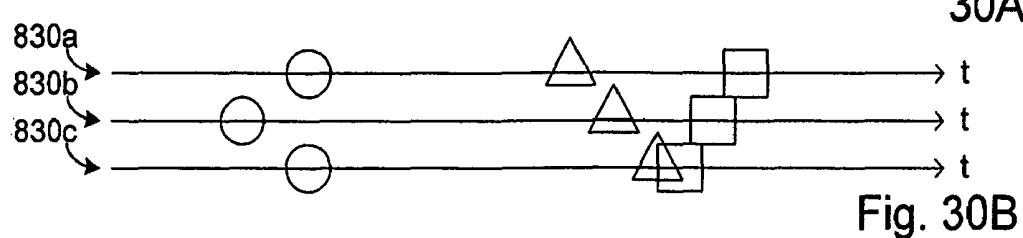
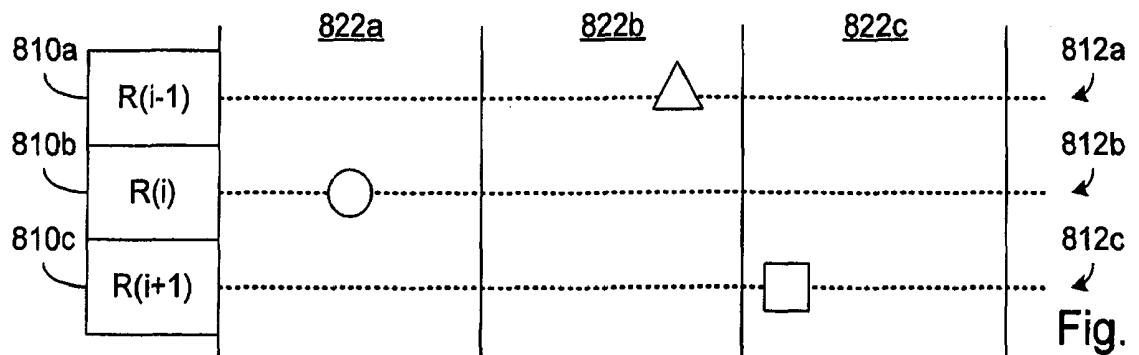


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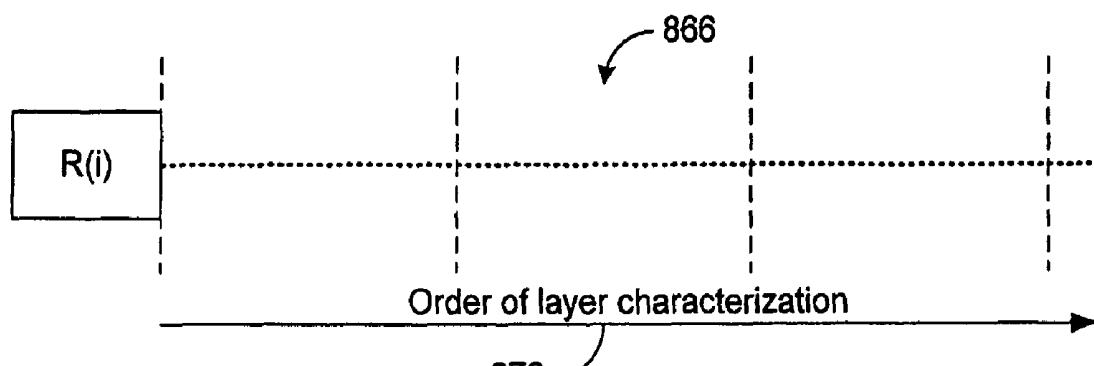


Fig. 31A

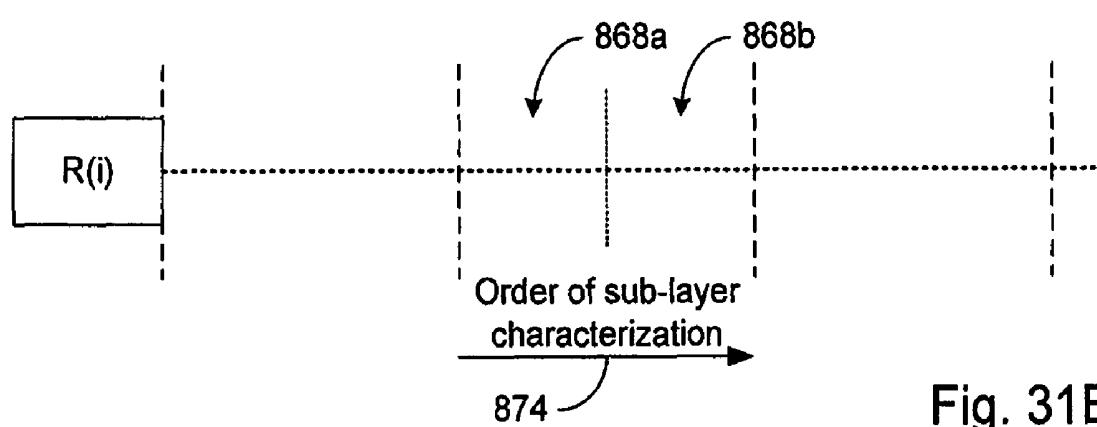


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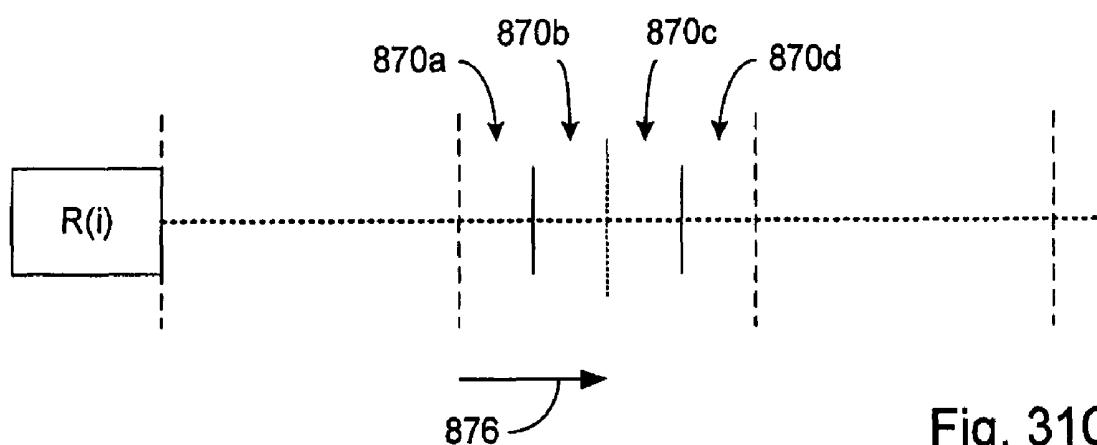


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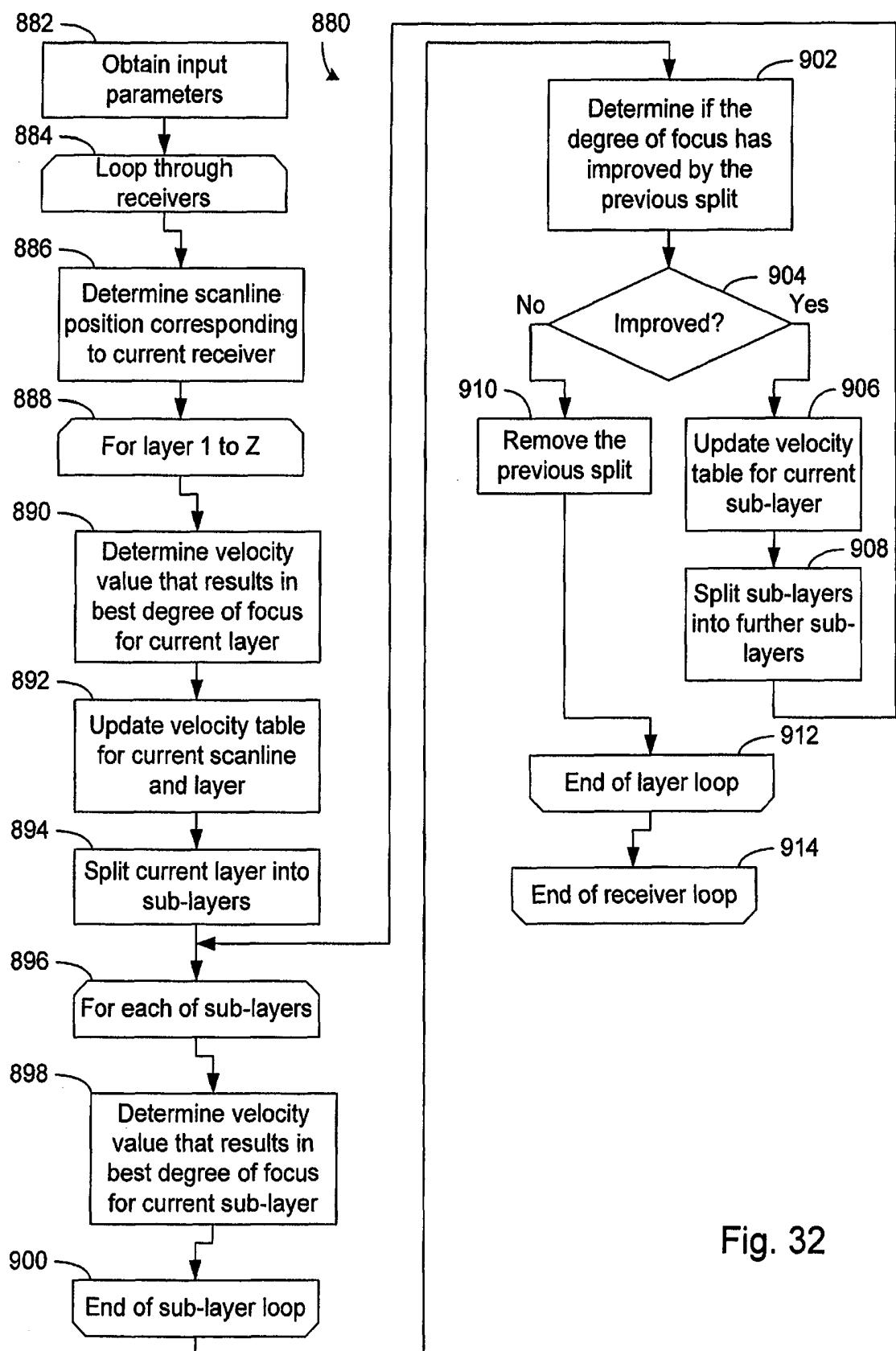


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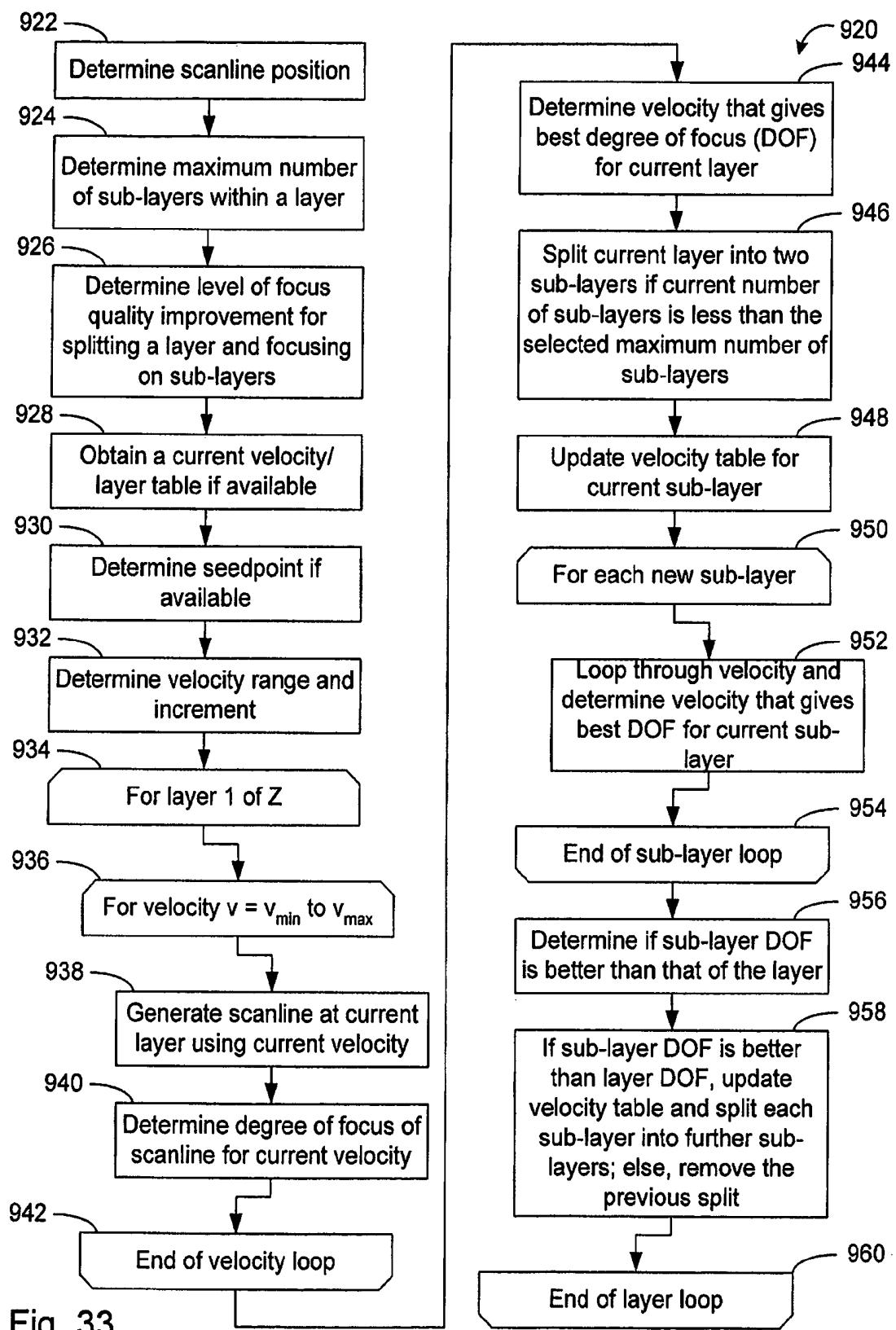
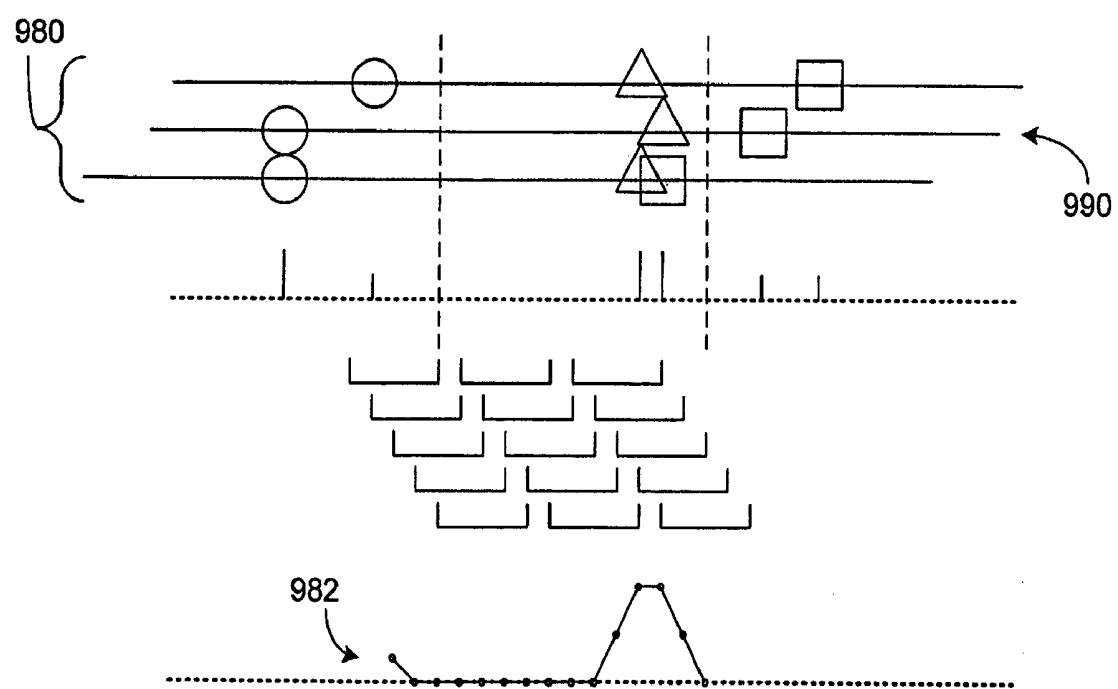
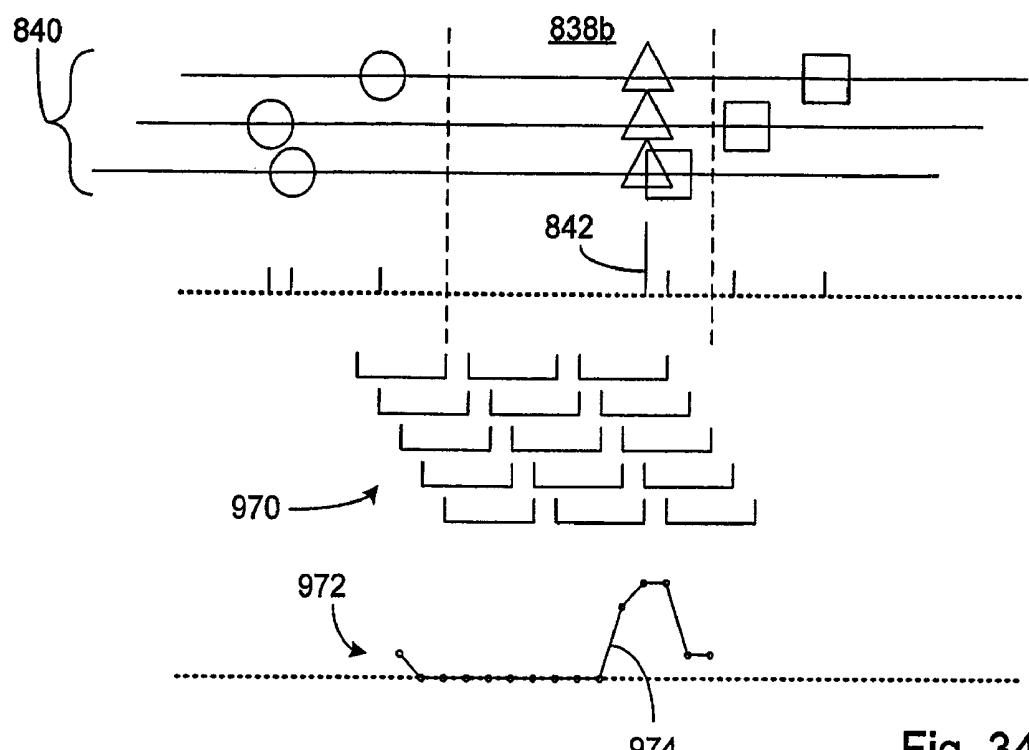


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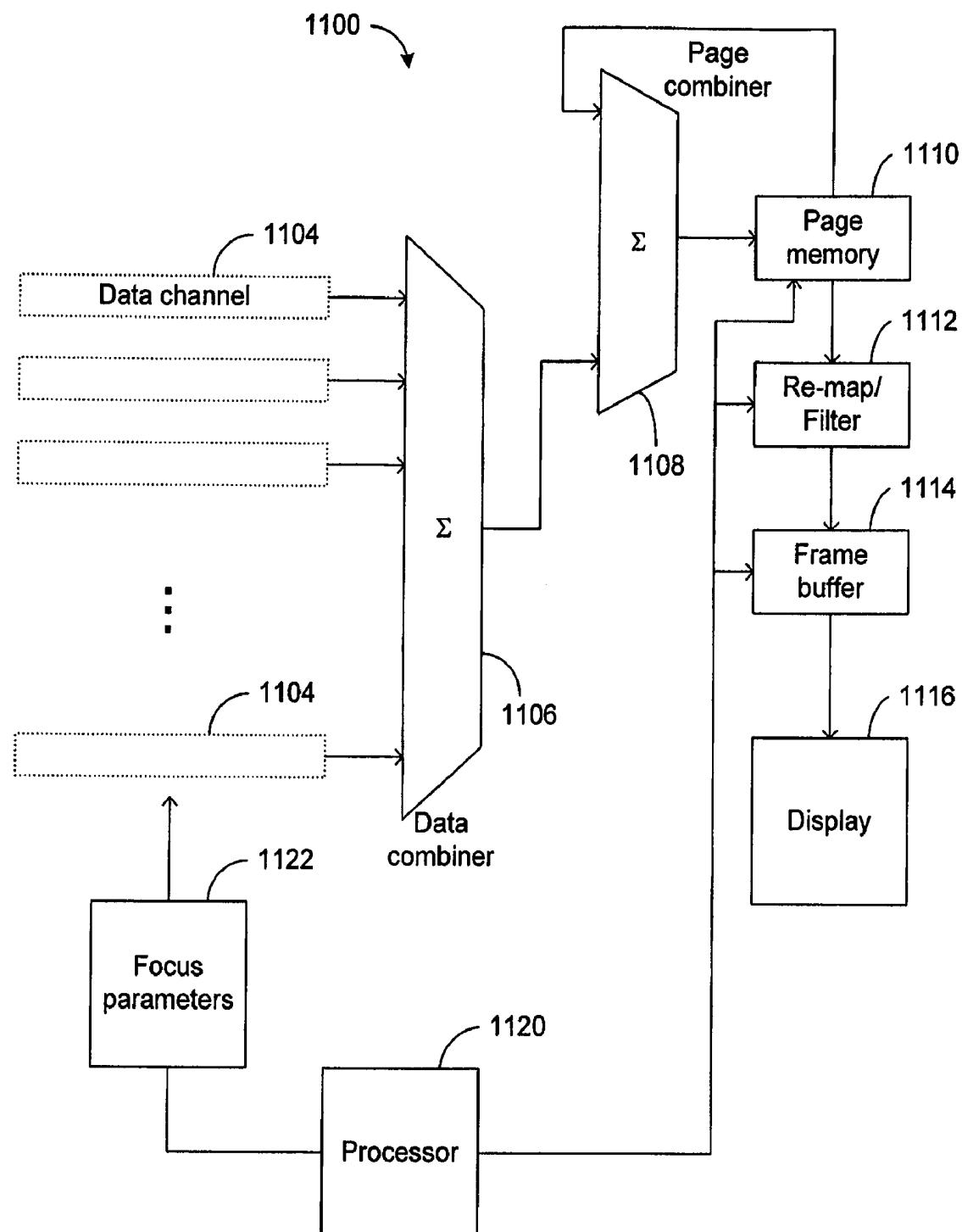


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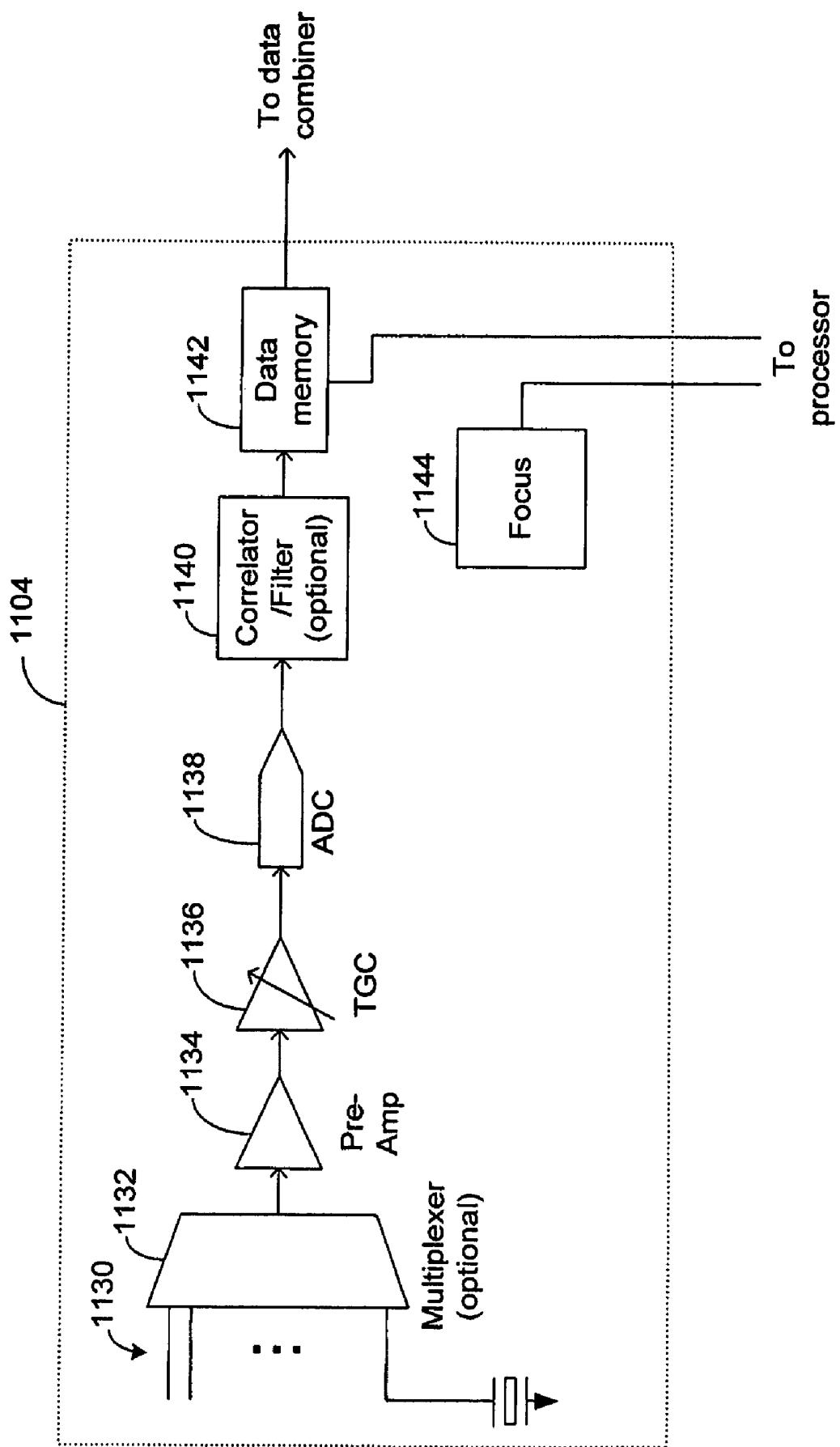


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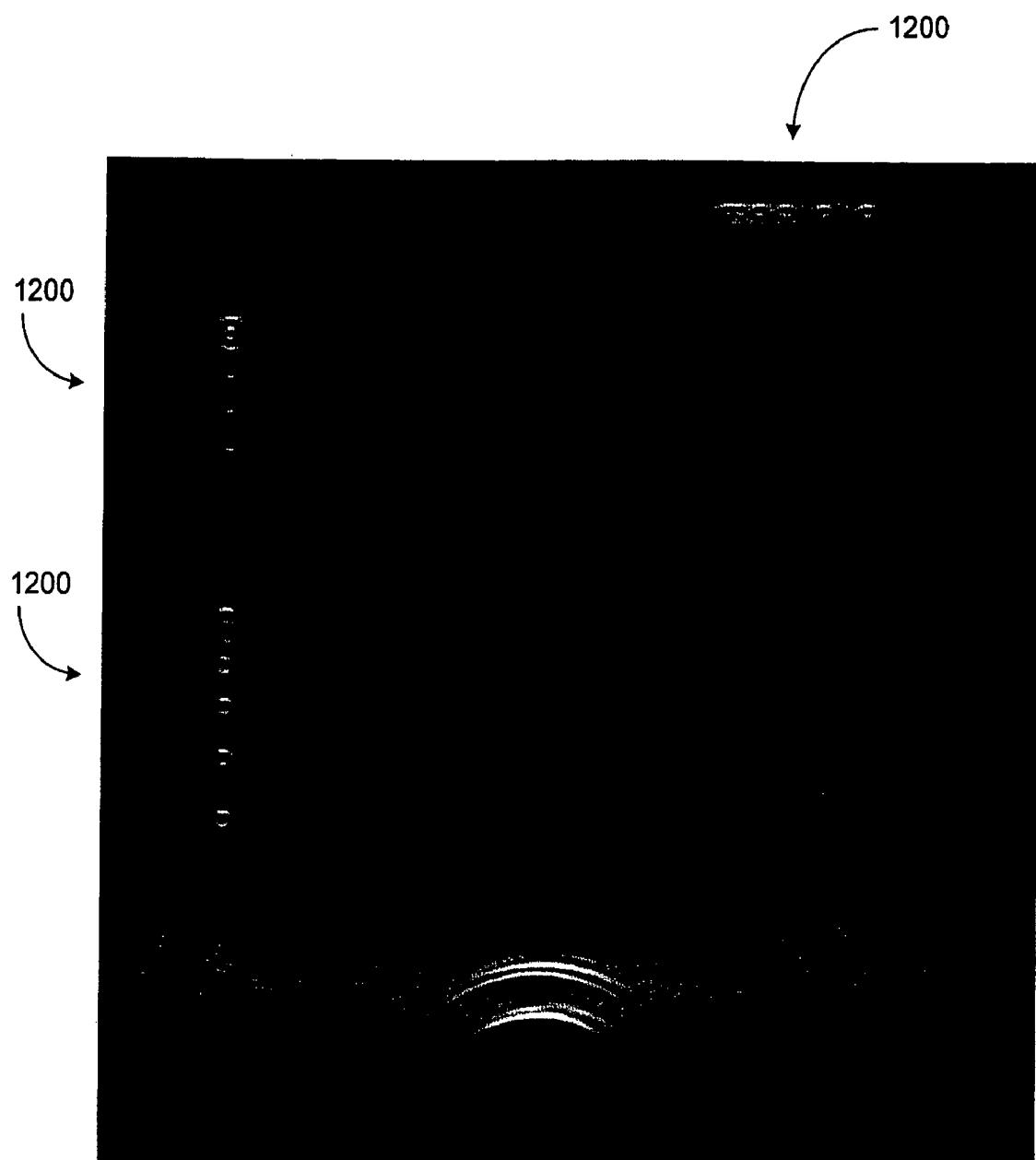


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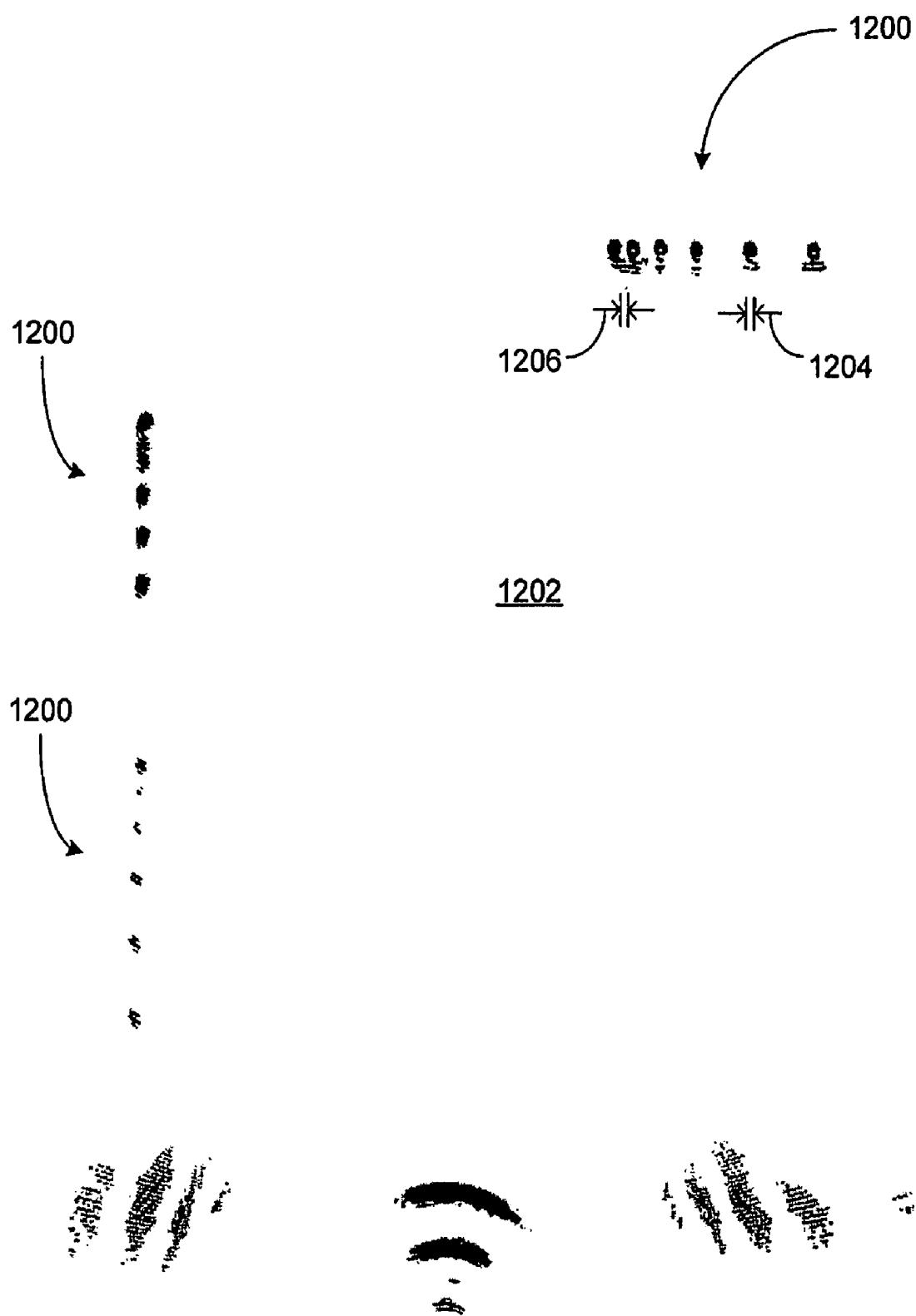


Fig. 36B

SYSTEM AND METHODS FOR IMPROVED ULTRASOUND IMAGING

BACKGROUND

1. Field

The present teachings generally relate to the field of imaging using waves and more particularly, to systems and methods for improving the resolution of images obtained by an array of transmitters and receivers.

2. Description of the Related Art

Imaging devices such as ultrasound devices transmit a signal into a medium, and measure reflections from various features in the medium. An image of a given feature can be reconstructed based on quantities such as intensity and frequency of the reflected signal from that feature. To form the image, one needs to somehow determine the relative location of the feature with respect to the imaging device, and in particular, to a location of a receiving element of the device.

Conventional ultrasound devices typically have an array of transmitter-receiver pairs. In operation, each pair only "sees" along a line, commonly referred to as a scanline, that extends from the pair into the medium. With such an assumption, a feature along that scanline can be brought into "focus" by determining the propagation times of the transmitted and reflected signals to and from the feature. A propagation time t can be calculated as $t=d/v$ where v is the velocity of the signal in the medium, and d is the distance of interest (e.g., from the feature to the receiver). The distance d can be determined by dividing the scanline into discrete elements in a predetermined manner, such that the location of each element is known. The velocity v can either be assumed as a constant in the medium, or can be calculated in a manner generally known in the art.

Based on such an operation, one can see that the resolution and quality of the image formed can be limited by the size of the scanline element. Even if the scanline element can be made arbitrarily small, the effective operation of and obtaining an image from the device is subject to the intrinsic resolution of the transmitter-receiver pair, as well as the sampling criteria for yielding a meaningful result.

The intrinsic resolution of a detector can be expressed as depending on the ratio of the operating wavelength of the signal to the effective dimension of the detector (commonly referred to as a Rayleigh or Sparrow criteria). One can change such a resolution of the detector by either changing the wavelength and/or the effective dimension of the detector. For example, reducing the wavelength (increasing the frequency) and/or increasing the effective dimension of the detector can improve the resolution. However, such a change can be accompanied by undesired effects. For example, an increased frequency signal has a smaller penetration depth in ultrasound applications.

Furthermore, an increased operating frequency also forces the minimum sampling frequency. Commonly known as the Nyquist sampling criteria, a signal needs to be sampled at a frequency that is at least approximately twice the frequency of the operating signal to yield a meaningful result.

Because of the foregoing challenges and limitations, there is an ongoing need to improve the manner in which imaging devices are designed and operated.

SUMMARY

The foregoing needs can be addressed by systems and methods for improving the resolution and quality of an image formed by signals from an array of receivers. Multiple receiv-

ers introduce variations in arrival times that can be less than the period of an operating signal, and also less than the period associated with a sampling operation. Thus, multiple receivers allow sampling of fine features of reflected signals that would be considered beyond the resolution associated with the operating signal. Use of multiple receivers also provides an effective sampling rate that is greater than the sampling rate of an individual receiver. Similar advantages can be obtained using multiple transmitters. Such advantageous features can be used to obtain high resolution images of objects in a medium in applications such as ultrasound imaging.

In some embodiments, the present teachings relate to a method of imaging an object in a medium with ultrasound. The method includes transmitting acoustic energy from a transmitter to the object such that the acoustic energy becomes scattered. The method further includes receiving the scattered energy at a plurality of receivers so as to produce respective analog echo signals. The method further includes sampling the analog echo signals at a frequency of F , with each of the sampled analog echo signals includes substantial spectral frequency components above a frequency of $F/2$. Such sampling produces a respective plurality of digital echo signals. The method further includes combining the plurality of digital echo signals, with each of the digital echo signals being offset by time with respect to another of the digital echo signals, so as to produce a combined digital signal that is selected from a plurality of different combinations of the plurality of digital echo signals. The method further includes producing an image pixel of the object from the combined digital signal.

In one embodiment, the method further includes producing a plurality of image pixels from the plurality of different combinations of the plurality of digital echo signals. The plurality of pixels distinctly depicts two objects in the medium that are closer together than $4F$ divided into an average velocity of sound in the medium. In one embodiment, such a method can distinctly depict two objects in the medium that are closer together than approximately 100 micrometers when the acoustic energy has a central peak frequency of approximately 3.5 MHz.

In one embodiment of the method, the substantial spectral frequency components above a frequency of $F/2$ include a higher frequency having an intensity that is above a predetermined value. Such a predetermined value can have different values, such as 50 dB, 40 dB, 30 dB, 20 dB, 10 dB, or 10 dB less than a maximum intensity of the spectral frequency components of one of the sampled analog echo signals.

In one embodiment of the method, the step of combining the plurality of digital echo signals includes selecting a first digital echo signal associated with a first receiver. The step further includes performing a plurality of time-shift combinations of the first digital echo signal with one or more digital echo signals associated with one or more other receivers about a selected time window of the first signal. Each of the plurality of combinations has a quality value indicative of a quality of the combination.

In one embodiment of the method, the step of combining the plurality of digital echo signals further includes assigning one of the plurality of combinations having a particular quality value to a scanline for the first receiver. In one embodiment, the selected time window corresponds to a layer having a first thickness along the scanline. In one embodiment, the particular quality value includes a running average of an amplitude of the one of the plurality of combinations. In one embodiment, the particular quality value includes a slope of a running average of an amplitude with respect to time of the one of the plurality of combinations.

In one embodiment of the method, the step of combining the plurality of digital echo signals further includes splitting a parent layer into two or more sublayers and performing time-shift combinations on each of the sublayers. The step further includes determining a best quality value for each of the sublayers. The step further includes comparing a best quality value of the parent layer to the best quality value of each of the sublayers. If the best quality value of the parent layer is substantially less than the best quality value of each of the sublayers, then the step further includes continuing to divide each of the sublayers into final sublayers, where each of the best quality values of the final sublayers is less than the best quality value of a parent layer of the final sublayers. In one embodiment, the step further includes assigning a combined digital signal of the parent layer of the final sublayers to the scanline.

In one embodiment of the method, the scanline is divided into a plurality of layers, and determinations of the particular qualities of the combinations are performed successively starting from a layer closest to the receiver.

In some embodiments, the present teachings relate to a method of imaging an object with ultrasound. The method includes providing an array of transmitters $Tx(i)$, where i represents a relative positional index that ranges from 1 to N , and where N is greater than or equal to 2. The method further includes providing an array of receivers $Rx(i)$, where each of the receivers $Rx(i)$ associated with a respective transmitter $Tx(i)$. The method further includes transmitting ultrasound energy from the transmitters to the object such that the ultrasound energy is scattered. The method further includes receiving scattered energy at every receiver $Rx(i+j)$ that was transmitted from transmitter $Tx(i)$, where j represents a relative positional offset from i , and where j is greater than zero. The method further includes generating a first plurality of signals in response to the scattered energies received at every receiver $Rx(i+j)$. The method further includes combining the plurality of signals so as to produce an image of the object.

In one embodiment the method, the value of j is one. In one embodiment, the method further includes receiving scattered energy at every receiver $Rx(i+k)$ that was transmitted from transmitter $Tx(i)$, where k represents a relative positional offset from i , and where k is greater than zero and is not equal to j . The method further includes generating a second plurality of signals in response to the scattered energies received at every receiver $Rx(i+j)$ and $Rx(i+k)$. The method further includes combining the first and second pluralities of signals so as to produce an image of the object.

In some embodiments, the present teachings relate to an ultrasound imaging apparatus that includes a plurality of transmitters configured to transmit acoustic energy to one or more objects in a medium such that the acoustic energy becomes scattered. The apparatus further includes a plurality of receivers configured to receive the scattered energy and in response produce respective analog echo signals. The apparatus further includes a processor that causes sampling of the analog echo signals at a frequency of F , where each of the sampled analog echo signals include substantial spectral frequency components above a frequency of $F/2$. The sampling produces a respective plurality of digital echo signals. The processor further causes combining of the plurality of digital echo signals, with each of the digital echo signals being offset by time with respect to another of the digital echo signals, so as to produce a combined digital signal that is selected from a plurality of different combinations of the plurality of digital echo signals. The processor further causes production of an image pixel of the object from the combined digital signal.

In one embodiment of the apparatus, the processor further causes production of a plurality of image pixels from the plurality of different combinations of the plurality of digital echo signals. The plurality of pixels distinctly depict two objects in the medium that are closer together than $4F$ divided into an average velocity of sound in the medium. In one embodiment, such an apparatus can distinctly depict two objects in the medium that are closer together than approximately 100 micrometers when the acoustic energy has a central peak frequency of approximately 3.5 MHz.

In one embodiment of the apparatus, the substantial spectral frequency components above a frequency of $F/2$ include a higher frequency having an intensity that is above a predetermined value. Such a predetermined value can have different values, such as 50 dB, 40 dB, 30 dB, 20 dB, 10 dB, or 10 dB less than a maximum intensity of the spectral frequency components of one of the sampled analog echo signals.

In one embodiment of the apparatus, the processor causes combining of the plurality of digital echo signals by a process that selects a first digital echo signal associated with a first receiver. The process further performs a plurality of time-shift combinations of the first digital echo signal with one or more digital echo signals associated with one or more other receivers about a selected time window of the first signal. Each of the plurality of combinations has a quality value indicative of a quality of the combination.

In one embodiment of the apparatus, the process further includes assigning one of the plurality of combinations having a particular quality value to a scanline for the first receiver. In one embodiment, the selected time window corresponds to a layer having a first thickness along the scanline. In one embodiment, the particular quality value includes a running average of an amplitude of the one of the plurality of combinations. In one embodiment, the particular quality value includes a slope of a running average of an amplitude with respect to time of one of the plurality of combinations.

In one embodiment of the apparatus, the process further includes splitting a parent layer into two or more sublayers, and performing time-shift combinations on each of the sublayers. The process further includes determining a best quality value for each of the sublayers. The process further includes comparing a best quality value of the parent layer to the best quality value of each of the sublayers. If the best quality value of the parent layer is substantially less than the best quality value of each of the sublayers, then the process continues to divide each of the sublayers into final sublayers. Each of the best quality values of the final sublayers is less than the best quality value of a parent layer of the final sublayers.

In one embodiment of the apparatus, the process further includes a combined digital signal of the parent layer of the final sublayers to the scanline. In one embodiment, the scanline is divided into a plurality of layers, and the determinations of the particular qualities of the combinations are performed successively starting from a layer closest to the receiver.

In some embodiments, the present teachings relate to an ultrasound imaging apparatus that includes a transducer assembly having a plurality of transmitting elements and a plurality of receiving elements. The plurality of transmitting elements are configured to transmit ultrasound energy, having a wavelength λ corresponding to a central peak frequency of the ultrasound energy, toward a region in a medium. The plurality of receiver elements generate a plurality of signals in response to scattered energy from the region. An aperture size D of the transducer assembly is the maximum distance between any two receiving elements in the transducer assem-

bly. The apparatus further includes a processor configured to sample the plurality of signals to produce a plurality of corresponding digital echo signals. The processor is further configured to combine the plurality of digital echo signals to generate an image having a spatial resolution limit that is equal to or better than $\theta = (0.25)\lambda/D$, where θ is the minimum resolvable angular separation of two objects in the medium.

In one embodiment of the apparatus, the spatial resolution limit allows resolving of two objects in the medium that are closer together than approximately 100 micrometers when the ultrasound energy has a central peak frequency of approximately 3.5 MHz. In one embodiment, the processor combines the plurality of digital echo signals by a process that includes selecting a first digital echo signal associated with a first receiver, and performing a plurality of time-shift combinations of the first digital echo signal with one or more digital echo signals associated with one or more other receivers about a selected time window of the first signal. Each of the plurality of combinations has a quality value indicative of a quality of the combination.

In one embodiment of the apparatus, the process further includes assigning one of the plurality of combinations having a particular quality value to a scanline for the first receiver. In one embodiment, the selected time window corresponds to a layer having a first thickness along the scanline. In one embodiment, the particular quality value includes a running average of an amplitude of the one of the plurality of combinations. In one embodiment, the particular quality value includes a slope of a running average of an amplitude with respect to time of the one of the plurality of combinations.

In one embodiment of the apparatus, the process further includes splitting a parent layer into two or more sublayers, and performing time-shift combinations on each of the sublayers. The process further includes determining a best quality value for each of the sublayers. The process further includes comparing a best quality value of the parent layer to the best quality value of each of the sublayers. If the best quality value of the parent layer is substantially less than the best quality value of each of the sublayers, then the process further includes continuing to divide each of the sublayers into final sublayers, where each of the best quality values of the final sublayers is less than the best quality value of a parent layer of the final sublayers.

In one embodiment of the apparatus, the process further includes assigning a combined digital signal of the parent layer of the final sublayers to the scanline. In one embodiment, the scanline is divided into a plurality of layers, and determinations of the particular qualities of the combinations are performed successively starting from a layer closest to the receiver.

In some embodiments, the present teachings relate to a method of imaging with ultrasound. The method includes transmitting ultrasound energy, having a wavelength λ corresponding to a central peak frequency of the ultrasound energy, from a plurality of transmitters in a transducer assembly into a medium such that the transmission energy is scattered. An aperture size D of the transducer assembly is the maximum distance between any two transmitters in the transducer assembly. The method further includes receiving scattered energies from the medium at a plurality of receivers. The method further includes digitally combining signals generated from the scattered energies so as to produce an image having a spatial resolution limit that is equal to or better than $\theta = (0.25)\lambda/D$, where θ is the minimum resolvable angular separation of two objects in the medium.

In one embodiment of the method, the spatial resolution limit allows resolving of the two objects in the medium that

are closer together than approximately 100 micrometers when the ultrasound energy has a central peak frequency of approximately 3.5 MHz. In one embodiment, the step of digitally combining the signals includes digitally sampling the signals so as to produce a plurality of digital echo signals. The step further includes selecting a first digital echo signal associated with a first receiver. The step further includes performing a plurality of time-shift combinations of the first digital echo signal with one or more digital echo signals associated with one or more other receivers about a selected time window of the first signal. Each of the plurality of combinations has a quality value indicative of a quality of the combination.

In one embodiment of the method, the step of digitally combining the signals further includes assigning one of the plurality of combinations having a particular quality value to a scanline for the first receiver. In one embodiment, the selected time window corresponds to a layer having a first thickness along the scanline. In one embodiment, the particular quality value includes a running average of an amplitude of the one of the plurality of combinations. In one embodiment, the particular quality value includes a slope of a running average of an amplitude with respect to time of the one of the plurality of combinations.

In one embodiment, the method further includes splitting a parent layer into two or more sublayers, and performing time-shift combinations on each of the sublayers. The method further includes determining a best quality value for each of the sublayers. The method further includes comparing a best quality value of the parent layer to the best quality value of each of the sublayers. If the best quality value of the parent layer is substantially less than the best quality value of each of the sublayers, then the method further includes continuing to divide each of the sublayers into final sublayers. Each of the best quality values of the final sublayers is less than the best quality value of a parent layer of the final sublayers. In one embodiment, the method further includes assigning a combined digital signal of the parent layer of the final sublayers to the scanline.

In one embodiment of the method, the scanline is divided into a plurality of layers, and determinations of the particular qualities of the combinations are performed successively starting from a layer closest to the receiver.

In some embodiments, the present teachings relate to a method of replicating information from a waveform energy emanating from an object over time, where the information includes a spectral frequency distribution having frequency components above a frequency $F/2$. The method includes digitally sampling the waveform energy at a temporal frequency of less than F to obtain sampled data. The method further includes producing a replica of the information from the sampled data, where the replica includes a spectral frequency distribution that substantially matches the spectral frequency distribution in a range below the frequency $F/2$. The energy is emitted from a plurality of emitters and is reflected from the object.

In one embodiment of the method, the energy is sampled with a plurality of detectors. In one embodiment, the energy is acoustic energy. In one embodiment, the energy is electromagnetic energy.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 shows a block diagram of one embodiment of an imaging system that images a defined volume in a medium;

FIG. 2 shows an example transmitter and an example receiver of one embodiment of an array forming an image associated with an example pixel of an image volume;

FIG. 3 shows a wave representation of an example array of transducers, where a transmitted signal from one example transducer is shown to reflect from an example target object such that the reflected wave can be detected by a plurality of receivers;

FIG. 4 shows how an image volume can be mapped into a plurality of pixels with respect to a plurality of transducers;

FIG. 5 shows an example of how a position of a pixel relative to a transmitter and a receiver can be stored independently as time-dependent indices based on their respective distances and wave propagation speed;

FIG. 6 shows how the indices can be used to selectively sample a signal received by a receiver;

FIG. 7 shows a process for obtaining a set of indices separately for transmitters and receivers for a given an array of pixels;

FIG. 8 shows a process for using the indices to selectively sample signals obtained by one or more receivers;

FIG. 9 shows an example of how a pixel array can be defined with respect to a transducer array, thereby allowing determination of distances between transducers and pixels;

FIG. 10 shows a process that separately determines indices corresponding to various position-defined transmitter-pixel and receiver-pixel combinations;

FIG. 11 shows a process that uses the transmitter-pixel and receiver-pixel indices to image selected pixels using selected transmitters and selected receivers;

FIG. 12 shows an example process that images a pixel array by transmitting from one selected transmitter and sampling from substantially all receivers;

FIG. 13 shows an example process that images a pixel array by transmitting from substantially all transmitters and sampling from one receiver;

FIG. 14 shows a ray representation of an example 32-transducer device being operated in a single-transmitter/all-receiver mode;

FIG. 15 shows a ray representation of the 32-transducer device being operated in an all-transmitter/single-receiver mode;

FIG. 16 shows how use of multiple receivers can allow sampling of fine perturbation features that are significantly smaller than that of a carrier signal;

FIG. 17 shows how signals from the multiples receivers can be combined to enhance a fine perturbation feature of interest;

FIG. 18A shows by example how a plurality of signals from receivers that are offset by one from their respective transmitters can be combined;

FIG. 18B shows by example how a plurality of signals from receivers that are offset by two from their respective transmitters can be combined;

FIG. 19 shows a process for transmitting from one or more transmitters and receiving from a plurality of receivers to allow combination of resulting signals;

FIG. 20 shows how the received signals from the plurality of receivers can be grouped according to the receivers' respective offsets from transmitters;

FIG. 21 shows how selected groups of data based on the receiver offset can be combined;

FIG. 22 shows an example of one embodiment of an array of transmitter-receiver pairs where the transmitters are triggered in sequence;

FIGS. 23A and B show a simplified depiction of example signal traces obtained from the example array of FIG. 22;

FIGS. 24A-F show a simplified depiction of example digitized data trace from the example signal traces of FIGS. 23A and B;

FIG. 24G shows an example of a combination of digitized data associated with receivers that are offset by one from their respective transmitters;

FIGS. 25A-F show a simplified depiction of example digitized data trace from the example signal traces of FIGS. 23A and B;

FIG. 25G shows an example of a combination of digitized data associated with receivers that are offset by two from their respective transmitters;

FIG. 26 shows how a signal from a given receiver can be combined with signal(s) from other receiver(s) to form a scanline for the given receiver such that the scanline has an improved performance for imaging a given layer;

FIG. 27 shows a plurality of scanlines intersecting with a layer such that the plurality of scanlines can be focused to that layer, and wherein the layer can be split into one or more thinner layers so as to allow finer focusing of the plurality of scanlines;

FIG. 28A shows an example of features located along different scanlines and in different layers;

FIG. 28B shows an example of measured signal traces having components associated with the example features of FIG. 28A;

FIGS. 28C-E show by example “in-focus” combinations at various layers for the signals traces to form the scanline associated with the first example receiver;

FIG. 29A shows an example of features located along different scanlines and in different layers;

FIG. 29B shows an example of measured signal traces having components associated with the example features of FIG. 29A;

FIGS. 29C-E show by example “in-focus” combinations at various layers for the signals traces to form the scanline associated with the second example receiver;

FIG. 30A shows an example of features located along different scanlines and in different layers;

FIG. 30B shows an example of measured signal traces having components associated with the example features of FIG. 30A;

FIGS. 30C-E show by example “in-focus” combinations at various layers for the signals traces to form the scanline associated with the third example receiver;

FIGS. 31A-C show that in one embodiment, a scanline can be focused from the layer closest to the receiver, and that a given layer can be split into finer layers for finer focusing;

FIG. 32 shows a process for focusing a plurality of scanlines in a plurality of layers, such that a given layer can be split for finer focusing if advantageous to do so;

FIG. 33 shows a more specific example of the process of FIG. 32;

FIGS. 34A-B show some of the many possible ways of combining various signal traces to obtain a best in-focus scanline at a given layer;

FIGS. 35A and B show by way of example one embodiment of a signal processing system that combines signals from the plurality of receivers;

FIG. 36A shows a photograph of an example of an actual image obtained using multiple receivers and combining signals therefrom in a manner described herein; and

FIG. 36B shows a negative image of the photograph of FIG. 36A.

These and other aspects, advantages, and novel features of the present teachings will become apparent upon reading the following detailed description and upon reference to the

accompanying drawings. In the drawings, similar elements have similar reference numerals.

DETAILED DESCRIPTION OF SOME EMBODIMENTS

The present teachings generally relate to systems and methods for forming an image of a portion of a medium. FIG. 1 shows a block diagram of one embodiment of an imaging device 100 that includes an array 110 of transducers. A transducer can represent a transmitter or a receiver. As is known, some transducers can operate as transmitters and as receivers. Thus for the purpose of description, a transducer can represent a transmitter, a receiver, or a combination thereof.

As shown in FIG. 1, the imaging device 100 further includes an array interface 112 that facilitates operation of the array 110 of transducers. The array interface 112 may, for example, multiplex and/or demultiplex a plurality of signals to and/or from transmitters and/or receivers. The transducer array 110 via the interface 112 may be supplied with a signal from a signal generator 114. The operation of the interface 112 in providing the signal to the array 110 and/or readout of the received signals from the receivers can be performed by a processor 116. As described below in greater detail, the processor 116 can operate the imaging device 100 in a manner that improves the resolution of the obtained image.

As shown in FIG. 1, the imaging device 100 further includes a storage device 118 that allows retrievable storage of various operating parameters in a manner described below. The imaging device 100 may further include a user interface 120 that provides an output for a user and/or allow a user to control some of the manner in which the imaging device 100 is operated.

As shown in FIG. 1, the imaging device 100 projects one or more signals into a medium 104 and detects responses of such transmitted signals therefrom. A region 102 that provides measurements in such a manner can be defined as an image volume 102. In the description herein, image volumes are sometimes represented as a two-dimensional plane. In many applications, image "planes" accurately describe the image volume. It will be understood, however, that such representation is in no way intended to limit the scope of the present teachings. It will also be understood that the shape and size of the image volume 102 may vary depending on factors such as the medium, the type of signal being used, and the properties of the imaging device.

It will also be understood that the imaging device, such as the device 100 of FIG. 1, may include both longitudinal-wave and transverse-wave devices. The longitudinal-wave device may include, but is not limited to, ultrasound-based devices, sonar-based devices, or devices that probe underground geological features. The transverse-wave device may include, but is not limited to, devices that operate based on electromagnetic waves such as optical devices or radar-type devices.

FIG. 2 now shows one embodiment of an example array 130 of transducers that images a volume 132. The example volume 132 can be defined by a plurality of corner locations 134a-h. Within the volume 132 is shown an example elemental volume 136 (also referred to as a pixel and/or voxel herein). A plurality of such pixels 136 make up the volume 132. It will be understood that the terms pixel (picture element) and voxel (volume element) are used interchangeably throughout the description.

In one embodiment, one or more transducers of the array 130 transmits one or more signals into the volume 132 so as to cover each of the pixels therein. A wave impinging on a pixel can be transmitted through the pixel, reflected from the

pixel, or any combination thereof. For example, if an object occupies the pixel, that object can cause a partial reflection and a partial transmission. Measurement of the reflected wave or lack of the reflected wave can yield an image of the pixel.

5 Thus as shown in FIG. 2, the example pixel 136 is depicted as being probed by a transmitted signal 138 from an example transmitter 142. The pixel's response to that signal 138 as measured by an example receiver 144 is indicated by a dashed arrow 140.

10 One can see that the resolution of an image of the volume depends on the size of the pixels, and the imaging device's ability to resolve such pixels. As described herein, one aspect of the present teachings relates to systems and methods of probing and measuring the pixels in a manner that improves 15 the resolution of images formed therefrom.

FIG. 3 shows an example waveform representation 150 of one embodiment of an array of transducers 154a-e probing a target object 160. In the example, the transducers 154 are shown to function as transmitters and receivers, and one receiver 152 is shown to transmit a signal 156. A waveform 158 impinges on the target 160 and reflects therefrom into a reflected wave 166. A propagated wave 164 is shown to be received first by the transducer 154c. The same waveform 164 would then be received by other transducers 154a, b, d, e at later times. Rays representing the reflected wave propagation towards the transducers 154a-e are indicated by dashed arrows 162a-e.

20 By synchronizing and combining the measurements of the reflected wave (example wave 164) by the various transducers, an improved image of the target can be formed. Although FIG. 3 shows a single-transmitter and multiple-receiver operation, it will be understood that any other combinations of transmitters and receivers can be used. As an example, the imaging device can be operated where multiple transmitters 25 transmit multiple signals that are measured by a single receiver. In another example, a plurality of transmitters and a plurality of receivers can be used in various combinations. One aspect of the present teachings relates to performing synchronization and combination of transmitters and/or receivers to improve the performance of the imaging device.

30 The imaging device can form an image of a portion of a medium containing one or more targets by defining that portion into a plurality of pixels. Thus, in the example target of FIG. 3 can occupy one or more pixels. Probing of those pixels, 35 along with other pixels, can yield an image of the target in its medium.

40 FIG. 4 shows one embodiment of an array of such pixels defined for an image plane 170. The image plane 170 is shown to be divided into an MxN array of pixels. Although FIG. 4 depicts the pixels as squares for the purpose of description; it will be understood that the pixels can be of any definable shape. Furthermore, the overall shape of the image plane 170 need not be rectangular shaped. Moreover, the image plane 170 is referred to as a "plane" for the purpose of description, and is not intended to limit the scope of the present teachings.

45 Some or all of the pixels of the image plane 170 can be probed by an array 172 of transducer elements. Such probing of the pixels is depicted by a plurality of arrows 174.

50 FIG. 4 shows L elements arranged along a line to form the array 172. It will be understood that the line arrangement of the transducer elements is for the purpose of description of the image plane 170. The array 172 of transducer elements can be arranged in a two-dimensional array, either in a planar manner or along some curved surface.

55 FIG. 5 now shows how a pixel 186 can be associated with a transmitter 182 and with a receiver 184. By performing such associations for all possible transmitter-pixel and receiver-

pixel combinations, a spatial and/or temporal alignment set (also referred to as an “alignment set” herein) of an array of pixels is obtained with respect to an array of transmitters and receivers. One aspect of the present teachings relates to mapping the pixels with respect to the transmitters separately from the receiver-pixel mapping. As described below, such a feature provides significant advantages during certain types of high-resolution imaging operations.

As shown in FIG. 5, the pixel 186 is positioned relative to the transmitter 182 by a distance d_{Tx} (as indicated by arrow 188). Similarly, the pixel 186 is positioned relative to the receiver 184 by a distance d_{Rx} (as indicated by arrow 190). The distance d_{Tx} can be used to determine when a signal from the transmitter 182 can be expected to reach the pixel 186. Similarly, the distance d_{Rx} can be used to determine when a possibly-reflected signal from the pixel 186 can be expected to reach the receiver 184. Such expectation information can be used to effectively combine signals associated with different transmitter-pixel and/or receiver-pixel combinations.

The expectation arrival information for the transmitter-pixel combination depends on the distance d_{Tx} , and can be represented as some form of an index. Such an index can also account for factors other than the distance that affect the arrival of the signal. As an example, electronic circuitry associated with the transmitter may cause the signal to be transmitted after a delay from some start time. Thus, an index data 194 corresponding to the distance d_{Tx} may also include such other factors.

Similarly, the expectation arrival information for the receiver-pixel combination depends on the distance d_{Rx} , and can be represented as some form of an index. Such an index can also account for factors other than the distance that affect the arrival of the signal. As an example, a readout process associated with the receiver may cause the signal to be sampled after a delay from the time when the signal impinges on the receiver. Thus, an index data 192 corresponding to the distance d_{Rx} may also include such other factors.

As shown in FIG. 5, the indices 194 and 192 can be stored independently in a retrievable storage 196. A collection of such indices for all possible transmitter-pixel and receiver-pixel combinations then defines the alignment set of the array of pixels.

FIG. 6 now shows how an alignment set for the pixel 186 can be used to obtain a selectively sampled signal 210 from an output 206 of the receiver 184. A transmitted signal from the transmitter 182 propagating towards the pixel 186 is depicted as an arrow 202. The signal 202 may or may not experience reflection from the pixel 186. Thus, an arrow 204 represents how a reflected signal would propagate from the pixel 186 to the receiver 184.

As further shown in FIG. 6, data 208 having the transmitter-pixel and receiver-pixel indices can be retrieved from the storage 196, and be used selectively sample the output 206 of the receiver 184. In one embodiment, such selectively sampled signal 210 is obtained by sampling the output 206 at an index corresponding to the sum of the transmitter-pixel and receiver-pixel indices. Some possible forms of the indices are described below in greater detail.

FIGS. 7 and 8 now show processes that perform the index determination and subsequent use, respectively, for an array of transducers. A process 220 determines the indices for a given pixel array with respect to a given array of transducers. The process 220 begins at a start state 222, and in a process block 224, the process 220 obtains detector and map parameters. Detector parameters may include the number of transmitters and the number of receivers. Map parameters may

include the number of pixels, the desired size of the pixels, and the arrangement of the pixels.

The process 220 in a process block 226 defines the array of transmitters and receivers. In one embodiment, each transmitter and each receiver are defined in terms of their positions relative to a chosen coordinate system. In an embodiment where transmitter and receiver function are performed by a common transducer, the array definition only needs to be performed for the transducer array. An example array definition is described below in greater detail.

The process 220 in a process block 228 defines the array of pixels as determined by the map parameters. In one embodiment, each pixel is defined in terms of its position relative to the transmitter/receiver array. An example array definition is described below in greater detail.

The process 220 in a process block 230 determines a propagation index corresponding to each transmitter-pixel combination. An example propagation index determination is described below in greater detail.

The process 220 in a process block 232 determines a sampling index corresponding to each receiver-pixel combination. An example sampling index determination is described below in greater detail.

The process 220 in a process block 234 stores the propagation indices and the sampling indices. An example storage of the indices is described below in greater detail. The process 220 ends at a stop state 236. In one embodiment, the alignment set generation process 220 is performed once for a given transducer array and a given pixel array, and does not need to be re-done during the imaging operation.

As shown in FIG. 8, an image generation process 240 determines the measured signals associated with some or all of the pixels using the previously determined alignment set for the transducer-pixel configuration. The process 240 begins at a start state 242, and in a process block 244, the process 240 obtains imaging parameters. In one embodiment, the imaging parameters include the number of transmitters and receivers, and alignment sets for transmitter-pixel and receiver-pixel combinations.

The process 240 in a process block 246 sets initial values for each of the pixels being evaluated. An example of such initialization is described below in greater detail.

The process 240 in a process block 248 transmits signal(s) into the pixel array, and samples signal(s) at indices corresponding to selected transmitter-pixel-receiver combinations. An example of selected transmitting and sampling is described below in greater detail.

The process 240 in a process block 250 determines the intensity of each of the selected pixels from the sampled signal(s). An example of such intensity determination is described below in greater detail.

The process 240 in a process block 252 processes the pixel intensities to form an image associated with the pixel array. The process 240 ends at a stop state 254.

FIGS. 9-11 now show more specific manner in which the transducer and pixel arrays can be configured, and how mapping and imaging operations can be performed on such a configuration. FIG. 9 shows an example configuration 260 of array of pixels 264 relative to an array of transducers 262. It will be understood that use of four example transducers 262 is for descriptive purpose only, and in no way intended to limit the scope of the present teachings. Similarly, the use of 5x6 array of pixels 264 is for descriptive purpose only, and in no way intended to limit the scope of the present teachings.

In one embodiment, the positions of the transducers 262 are defined with respect to a coordinate system 266. Although

a Cartesian coordinate system is used, it will be understood that any coordinate system can be used for such definition.

In one embodiment, the array of pixels 264 are formed by dividing up an image plane into a grid (5×6 in the example) of pixel regions. One way to define such a grid is to define the positions of set of opposing corner pixels—for example, (1,1) and (5,6), or (1,6) and (5,1), with respect to the coordinate system 266. Then, one can specify number of rows (5 in this example) and columns (6 in this example). Such a definition of the grid provides sufficient information to define the size and position of each of the pixels. One can see that the pixel grid can be defined in any number of ways. Thus, the example method disclosed herein is not intended to limit the scope of the present teachings.

Once the pixel grid 264 is established with respect to the chosen coordinate system 266, each pixel's position can be referenced to each transducer. As an example, the pixel (2,3) is shown to be referenced to transducers 1 to 4 as denoted by arrows 268a-d. Such relative positions of the pixel to the transducers can be used to obtain the transmission indices and sampling indices.

One way of obtaining an index associated with a given transducer-pixel combination is to first determine the distance between the transducer and the pixel. Such determination can be achieved by simple geometry calculation based on the chosen coordinate system. As an example, if the coordinates of the pixel and the transducer can be represented by (x_p, y_p, z_p) and (x_t, y_t, z_t) respectively, the distance d between the two points can be calculated as square root of the quantity $(x_t - x_p)^2 + (y_t - y_p)^2 + (z_t - z_p)^2$.

The distance d obtained in the foregoing manner can then be used to determine the propagation time t between the transducer and the pixel as $t = d/v$ where v is the magnitude of the propagation velocity of the signal of interest in the medium. For sampling purposes, the propagation time t can further be expressed as a sample number i_{sample} for situations where the received signal is sampled at a sampling rate. In one embodiment, the sample number can be represented as $i_{sample} = (t)(\text{sample rate})$. As previously described, the actual time between some “start” time and sampling time may include time(s) in addition to the propagation times. Such additional time, if any, can also be represented as a sample-rate-based quantity, and added to that associated with the propagation times.

From the foregoing description of the sample number determination, one can see that similar information can be obtained in any number of ways. Thus, it will be understood that any number of other methods, or variations of the disclosed method, can be used to obtain and store the indices associated with the transmitter-pixel and receiver-pixel combinations.

FIG. 10 now shows one implementation of a detailed process 270 for determining an alignment set for a given pixel array with respect to given transmitter and receiver arrays. The process 270 begins at a start state 272, and in a process block 274, the number of transmitters is determined. In a process block 276, the number of receivers is determined. In a process block 278, the position of each transmitter is determined. In a process block 280, the position of each receiver is determined.

In a process block 282, the process 270 defines an image plane by determining positions of two opposing corners of the image plane. In a process block 286, the image plane is divided into a grid defined by desired numbers of rows and columns of pixels.

In a process block 288, the process 270 determines the signal's velocity through the medium being imaged. In a process block 290, the sampling rate is determined.

As shown by a loop 292 (with end-loop 308), the process 270 loops through the transmitters. For each transmitter, the process 270 loops through the pixels (loop 294, with end-loop 306). Thus for each combination of the transmitter and pixel, the process 270 determines the pixel position in a process block 296. In a process block 298, the distance between the transmitter and the pixel is determined. In a process block 300, propagation time between the transmitter and the pixel is determined based on the distance and signal velocity ($t = d/v$). In a process block 302, an index corresponding to the propagation time is determined. In one embodiment, the index can be represented as a product of the propagation time and the sampling rate of the imaging device. In a process block 304, the index corresponding to the transmitter-pixel combination is saved for later retrieval and use. The loops 294 and 292 end at loop-ends 306 and 308 respectively.

As shown by a loop 310 (with end-loop 326), the process 270 loops through the receivers. For each receiver, the process 270 loops through the pixels (loop 312, with end-loop 324). Thus for each combination of the receiver and pixel, the process 270 determines the pixel position in a process block 314. In a process block 316, the distance between the receiver and the pixel is determined. In a process block 318, propagation time between the pixel and the receiver is determined based on the distance and signal velocity ($t = d/v$). In a process block 320, an index corresponding to the propagation time is determined. In one embodiment, the index can be represented as a product of the propagation time and the sampling rate of the imaging device. In a process block 322, the index corresponding to the receiver-pixel combination is saved for later retrieval and use. The loops 312 and 310 end at loop ends 324 and 326 respectively. The process 270 ends at a stop state 328.

As previously described, the alignment set generation, such as that of the process 270, is generally performed once and does not need to be repeated during subsequent imaging operations. The stored indices corresponding to the transmitter-pixel and receiver-pixel combinations allow such subsequent improved-resolution imaging operations to be performed in an efficient manner.

FIG. 11 now shows one implementation of a detailed process 330 for performing an imaging operation utilizing the alignment set obtained previously. The process 330 begins at a start state 332, and in a process block 334 an operating configuration of transmitters, receivers, and pixels is determined. In one embodiment, such an operating configuration defines the numbers and positions of the transmitters, receivers, and pixels in a manner similar to that used for the alignment set determination process. As such, one or more operating configurations can be stored, and one configuration can be either selected by a user or be used as a default.

In a process block 336, the process 330 obtains a set of indices corresponding to the transmitter-pixel combinations of the operating configuration. In a process block 338, a set of indices corresponding to the receiver-pixel combinations of the operating configuration is obtained.

In a process block 340, the process 330 initializes the imaging detector. In one embodiment, such initialization includes initializing the values of the pixel intensities.

In a process block 342, the process 330 transmits a signal from selected transmitter(s) and begins sampling for return signals from the pixel array using selected receiver(s). In one embodiment, a sampling “start” is issued at some predetermined time about the time when the signal leaves the transmitter. Referencing the samplings from such a common start

time allows correlated sampling of all the transmitter-pixel-receiver combinations. By having separate sets of transmitter-pixel and receiver-pixel indices, such correlated sampling, as well as other variations of operation of the imager, can be performed more efficiently.

In one embodiment, the process 330 measures the pixel array by sampling signals associated with each of the transmitter-pixel-receiver combinations. One way to cover all the combinations is to perform nested loops for the transmitters, pixels, and receivers. Thus, the process 330 is shown to loop through the selected pixels (loop 344, end-loop 364). For each pixel in the pixel loop 344, its intensity value is initialized in a process block 346. For each initialized pixel, the process 330 loops through the selected transmitters (loop 348, end-loop 362). For each pixel-transmitter combination, the process 330 loops through the selected receivers (loop 350, end-loop 360). Thus for each pixel-transmitter-receiver combination of the nested loops 344, 348, 350, the process 330 in a process block 352 obtains a signal from the current receiver. In a process block 354, the index for the current transmitter-pixel combination is obtained. In a process block 356, the index for the current receiver-pixel combination is obtained. In a process block 358, the pixel intensity is adjusted by a value of the receiver signal corresponding to the sum of current transmitter-pixel and receiver-pixel indices.

As shown in FIG. 11, pixel intensity values obtained in the foregoing manner can be further analyzed or stored (for later analysis) in a process block 366. The process 330 ends in a stop state 368.

FIGS. 12 and 13 now show two specific examples of using selected transmitter(s) and selected receiver(s) to obtain an improved image quality. In FIG. 12 an example process 370 is shown where a single selected transmitter and a plurality of selected receivers are used. In FIG. 13, an example process 400 is shown where a plurality of selected transmitters and a single selected receiver are used.

As shown in FIG. 12, the example process 370 in a process block 372 transmits a signal from a selected transmitter and begins sampling. Such a beginning of sampling can be at a predetermined time relative to the time when the transmitted signal begins propagating from the transmitter. The process 370 then loops through all of the pixels in a loop 374 (with an end-loop 390). For each pixel, the process 370 sets that pixel's initial value to zero in a process block 376. Also for that pixel, the process 370 obtains the index i_{Tx} for the current transmitter-pixel combination in a process block 378.

For the current pixel, the process 370 then loops over all of the selected receivers in a loop 380 (with an end-loop 388). The process 370 in a process block 382 obtains a signal S from the current receiver. In a process block 384, the index for the current pixel-receiver combination i_{Rx} is obtained. In a process block 386, the current pixel's intensity value is adjusted as $I=I+S(i_{Tx}+i_{Rx})$.

As shown in FIG. 13, the example process 400 in a process block 402 transmits signals from all of the selected transmitters, and begins sampling from one selected receiver. Transmitting of the signals from the selected transmitters can be either simultaneous or in a predetermined sequence. In embodiments where the number of selected transmitters is relatively small, the signals may be transmitted substantially simultaneously, and the sampling may be able to temporally distinguish the transmitter-pixel-receiver combinations. In embodiments where the number of selected transmitters is relatively large, the signals being transmitted simultaneously may not allow effective selective sampling of the transmitter-pixel-receiver combinations.

In embodiments where the signals are transmitted simultaneously, beginning of sampling can be at a predetermined time relative to the time when the transmitted signals begin propagating from the transmitters. In embodiments where the signals are transmitted in some sequence, beginning of sampling can be defined in a variety of ways. One way is to have a common start time, and account for the different transmit times for different transmitters as adjustments to the transmitter-pixel combination indices.

10 The process 400 then loops through all of the pixels in a loop 404 (with an end-loop 420). For each pixel, the process 400 sets that pixel's initial value to zero in a process block 406. Also for that pixel, the process 400 obtains the index i_{Rx} for the current receiver-pixel combination in a process block 408.

15 For the current pixel, the process 400 then loops over all of the selected transmitters in a loop 410 (with an end-loop 418). The process 400 in a process block 412 obtains a signal S from the receiver. In a process block 414, the index for the current transmitter-receiver combination i_{Tx} is obtained. In a process block 416, the current pixel's intensity value is adjusted as $I=I+S(i_{Tx}+i_{Rx})$.

20 In one embodiment as shown in FIG. 14, an imaging device includes 32 elements. In particular, FIG. 14 shows a ray representation 500 of the embodiment where one transmitter (transmitter 16) transmits a signal 506 to an object 504, resulting in a reflected wave 510 that is detected by 32 receivers (1 to 32). The reflected wave 510 propagating to the receivers 502 is represented by reflected rays 508, and the intersection 25 of the wavefront 510 with the rays 508 represent the in-phase portions of the rays 508.

25 For the example embodiment 500, the index i_{Tx} representative of the transmitted signal 506 is common to all of the sampling indices used by the 32 receivers. For the particular example where the object is located at the mid-level of the array 502, the reflected wave 510 reaches receiver 16 first. Thus, the sampling index associated with the pixel where the object 504 is located would have a value that causes the signal from receiver 16 to be sampled first. Thereafter, signals from 30 receivers 15 and 17 would be sampled, followed by 14 and 18, etc. Signal from receiver 32 would be the last to be sampled at a time corresponding to the extra propagation distance of the wavefront 510.

35 In one embodiment as shown in FIG. 15, an imaging device includes 32 elements. In particular, FIG. 15 shows a ray representation 520 of the embodiment where all 32 transmitters transmit signals 526 to an object 524, resulting in a reflected signal 528 that is detected by receiver 16. For the example embodiment 520, the index i_{Rx} representative of the reflected signal 528 is common to all of the sampling indices associated with the 32 receivers.

40 For the particular example where the object is located at the mid-level of the array 502, the transmitted signal from transmitter 16 reaches the object 524 first (assuming that all signals are transmitted simultaneously). Thus, the sampling index associated with the pixel where the object 524 is located would have a value that causes the first sampled signal to be associated with transmitter 16. The next set of sampled signals would be associated with transmitters 15 and 17, and so on. The last set of sampled signals would be associated with transmitter 32.

45 As previously described in reference to FIG. 13, the plurality of signals can be transmitted from the transmitters in different ways. Sequenced transmission of signals from the plurality of transmitters can temporally separate the arrivals of the signals at the object 524, as well as reflected signals at the receiver thereafter. One way to sequence the signal trans-

mission is to begin transmission at the transmitter 16, followed at a predetermined time by transmission at transmitters 15 and 17, etc. Such a sequence of transmission can increase the temporal separation of the samplings associated with the array of receivers 522.

FIG. 16 now shows how sampling by a plurality of transducers can yield an effective sampling rate that is greater than a sampling rate associated with each of the transducers. In an example operating configuration 600, a transmitter 602 is depicted as transmitting a transmission energy 604 into a medium (not shown) in response to a transmission signal 606. The transmission signal 606 is depicted as a periodic signal; but such a characteristic is not a requirement. The transmission signal 606 can be of any waveform having some time-characterizable feature. For example, if the transmission signal 606 is a single pulse, it may be characterized by its temporal width.

The example operating configuration 600 further includes a plurality of receivers 610 that receive respective reflection energies 612. In response to the reflection energies 612, the receivers 610 output respective signals 614 that are sampled. In this example, the plurality of receivers 610 are shown to be sampled simultaneously for the purpose of description. It will be understood that simultaneous sampling of the receiver signals is not a requirement.

Also for the purpose of description, the common sampling is shown to have a period $T_{sampling}$ that is approximately half of the transmission signal period T_{signal} . As such, the sampling frequency in such a situation is approximately twice the transmission signal frequency. In general, a sampling frequency should be at least twice the frequency of a signal being analyzed to be able to characterize that signal; and the “twice” lower limit is often referred to as the Nyquist limit.

As shown in FIG. 16, the example signals 614 output by the receivers 610 are shown to have an underlying “carrier” signal structure (dotted curve superimposed for descriptive purpose) that can have a similar structure as the transmission signal 606. The signals 614 can include a plurality of perturbations about the carrier signal structure. Such perturbations can be the result of the interaction of the transmission signal 606 with some feature of interest in the medium, or due to background noise. Whatever the cause may be, such perturbations may have (and are depicted as having) sub-wavelength feature sizes when compared to the carrier signal structure or the sampling period. As such, sampling of an individual receiver alone will not be able to resolve the fine-feature structures associated with noises or legitimate signals.

When a plurality of receivers are used, the receivers may be arranged so that reflected energies arrive at the receivers at different times. Such arrival time differences can be caused by differences in propagation times due to the pathlength differences and/or velocity differences caused by medium anisotropy. In FIG. 16, such an arrival difference is depicted as ΔT for the receivers 610a and 610b. For a given pair of receivers, the arrival difference ΔT can be made substantially smaller than the sampling period $T_{sampling}$ or the transmission signal period T_{signal} .

With an array of receivers, successive arrival differences can be introduced to the receivers. Then, a common sampling of the receivers can have an effect of having the individual receivers sampling different temporal parts of the received signals. Thus in the example configuration 600, the common sampling at time t_1 causes the example signal 614c (that arrives late) to be sampled at a given temporal part of the carrier structure (beginning of the cycle in the example). Sampling at time t_1 causes the example signal 614b to be sampled at a temporal part of the carrier structure at a time

approximately equal to the arrival difference between the receivers 610b and 610c. Similarly, sampling at time t_1 causes the example signal 614a to be sampled at a temporal part of the carrier structure at a time that is approximately equal to the arrival difference between the receivers 610a and 610b. When the samplings from the receivers 610a, b, and c are combined, the resulting measurement can be equivalent to sampling at intervals of arrival difference ΔT that is substantially smaller than the common sampling interval of $T_{sampling}$.

One can see that the number of receivers and/or the arrival time difference can be selected so that the effective sampling intervals are distributed between two common sampling intervals (for example, between common sampling times t_1 and t_2 in FIG. 16). Thus, with proper configuration, an array of receivers can be used to sample the received signals at a frequency that is greater than the common sampling frequency, thereby be able to resolve higher frequency (than the transmission signal frequency) perturbation signal components that are “riding” on the carrier signal structure.

To be able to extract the higher frequency perturbation features, it is preferable in one embodiment to not filter the received signals. In some conventional systems, filtering is used to remove these higher frequency perturbations. Such filtering, however, can filter out a perturbation that is caused by an interaction of interest along with the noise perturbations.

One can see that sampling the received signals at a effectively higher frequency as described above is one aspect of achieving an improved imaging. Such sampling samples both the perturbations of interest and noise. Thus, another aspect of improved imaging includes a method of combining the samplings from different receivers so that the signal to noise ratio of the sampled perturbations is increased.

FIG. 17 shows an example of how combination of the samplings from a plurality of receivers can enhance a relatively weak signal from a reflection of interest from the medium. A plurality of example segments of signals 620 are shown superimposed to a carrier signal (dotted curve 622). Each of the example signal segments 620 is shown to include a relatively weak signal of interest 626 among its own set of noise structures. Each signal may have different noise structures since the signal is representative of a path that is different from other signals. If any perturbation within the signal is present in at least some significant portion of the plurality of signals 620, such a perturbation is likely due to some interaction of interest in the medium, and are likely correlated among the signals.

As described above in reference to FIG. 16, such relatively fine-featured perturbations, whether a legitimate signal or noise, are more likely to be sampled with the effective sampling rate that can be substantially greater than that of the common sampling frequency. Thus, an example of a plurality of such effective samplings are depicted as dashed lines 624. It should be understood that the effective sampling lines 624 in FIG. 17 are shown only for the purpose of demonstrating that when properly correlated, the plurality of signals 620 can yield an enhancement of the perturbation of interest over the surrounding noise perturbations. A method of forming such a correlation of signal samplings is described below in greater detail.

It should also be understood that the perturbation of interest 626 in FIG. 17 is depicted as being sampled near the peak for the purpose of description. Because the arrival differences (ΔT s) among the receivers may not be uniform, spacing between the effectively increased samplings may not be uniform. Consequently, samplings of the perturbation 626 may be at different parts of the perturbation peak structure. In one

embodiment, such an effect limits the resolution achievable by the effectively increased sampling.

In one embodiment, properly correlated analog signals from the selected receivers can be made to interfere with each other. In such an embodiment, the various analog signals can be provided with delays according to the manner in which the signals are correlated.

In one embodiment, the raw signals from the selected receivers are digitized during the common samplings. The plurality of receivers and their associated sampling electronics are then effectively sampling and digitizing different temporal portions of their respective signals. As shown in FIG. 17, the digitized results are shown to be correlated and combined so as to yield a combined data sequence 628. When the digitized results of the signals are combined properly, individual digitized values of the perturbation of interest 626 combine to yield an enhanced digitized value 630. In contrast, the sampled and digitized noises either combine to generally cancel each other on average, or combine in a manner that is less than that of the correlated perturbation value 630.

In principle, the combining of the signals can be performed with any receivers in the array. However, Applicant's experiences have shown that correlating and combining signals from some combinations of transmitter and receivers yield better results in the quality of images.

FIGS. 18A and 18B show two examples of such transmitter-receiver combinations. In FIG. 18A, an example operating configuration 640 has an i-th transmitter 642a transmitting an energy 646, and a receiver (i+1) 644b that is offset by one element spacing receiving a reflected signal 648 (from an arbitrary point 658 in the medium) and generating a signal. Thus, an energy 650 from a transmitter (i+1) 642b is reflected as an energy 652 and received by a receiver (i+2) 644c. Similarly, an energy 654 from a transmitter (i+2) 642c is reflected as an energy 656 and received by a receiver (i+3) 644d. In one embodiment, such transmit-receive combination between transducers offset by one unit provides a substantially "head-on" type of probing of the arbitrary point 658 in the medium.

In FIG. 18B, an example operating configuration 660 has the i-th transmitter 642a transmitting an energy 662, and the receiver (i+3) 644c that is offset by two element spacing receiving a reflected signal 664 (from the arbitrary point 658 in the medium) and generating a signal. Thus, an energy 666 from the transmitter (i+1) 642b is reflected as an energy 668 and received by the receiver (i+3) 644d. Such an offset can provide a more angled probing of the point 658 in the medium.

One can see that such offset pairing of the transmitter and receiver can extend to three, four, or greater offset units. In principle, any offset in the array can be used. In some applications, such a capability can be used to investigate reflections and/or emissions from a given object that are directed towards sidelobe angles.

FIGS. 19-21 now show various processes that perform the sampling and combining of signals from different transmitter-receiver offsets. FIG. 19 shows one embodiment of a process 680 that transmits from selected transmitters in a sequential manner. In one embodiment, a master time reference is designated in a process block 682. Such a master time can be used for referencing subsequent time-related operations. The process 680 then loops through the selected transmitters (begin loop 684, and end loop 694). In a process block 686, the process 680 induces the current transmitter to transmit energy into the medium. In a process block 688, the return signals are received from selected receivers. In one embodiment, all of the receivers receive return signals impinging on

them. In a process block 690, the process 680 samples and stores the resulting data from the selected receivers. In one embodiment, the process 680 may wait for a selected duration before transmitting from the next transmitter.

FIG. 20 now shows one embodiment of a process 700 that combines the sampled data according to different transmitter-receiver offset groups. The process 700 loops through different values of offset N between the transmitter and the receiver of interest (begin loop 702, end loop 708). In one embodiment, the value of offset N ranges from zero to N_{max} , with N=0 representing a case where the receiver is in the same assembly as the transmitter. In a process block 704, the process 700 forms a "page" of data by combining data from receivers that are offset by the current value of N from the selected transmitters. In a process block 706, the process stores the page of data corresponding to the current offset value of N.

FIG. 21 now shows one embodiment of a process 710 that uses the page(s) of data to characterize the medium. In a process block 712, the process 710 retrieves selected page(s) of data corresponding to transmitter-receiver offset value(s) of N. In a process block 714, the process 712 combines the selected page(s) to characterize the medium. In one embodiment, characterization of the medium includes formation of an image of the medium.

FIGS. 22 to 25 now show a specific example of the data page formation based on the offset of the transmitter and receiver pairs. For the purpose of describing by example, an example operating configuration 730 having six sets of transmitter-receiver assemblies 732 are shown in FIG. 22. It will be understood that such a configuration is only for descriptive purpose, and is not in any way intended to limit the scope of the present teachings.

In one embodiment, each transmitter-receiver assembly includes a transmitter (Tx) and a receiver (R) positioned in a close proximity to the transmitter. As depicted by an arrow 734, the six example transmitters (Tx1 to Tx6) are "fired" in sequence, starting from the first transmitter Tx1.

Also shown in FIG. 22 is an arbitrary point 736 in the medium. In one embodiment, a given transmitter does not transmit until return signals from the medium, including the point 736, would have had time to return to all of the receivers. It will be understood that the arbitrary point 736 is shown to aid in the purpose of description, and a-priori knowledge or assumption of its location with respect to the array 732 is not required.

FIGS. 23A and 23B now show examples of simplified raw analog traces from the six example receivers of FIG. 22 in response to receiving of reflected signals due to a given transmitter. For the purpose of describing how a particular perturbation peak can be at different temporal portions of different traces, the traces are depicted to only show the peak. It should be understood that there will likely be other perturbation features in the traces, as described above in reference to FIGS. 16 and 17.

FIG. 23A shows example traces 750 associated with transmission from Tx1. In one embodiment, each of the traces 750 are sampled between a "Start" time and a "Stop" time while being referenced to a master time reference. Thus, if the perturbation peak is assumed to originate from the point 736 in FIG. 22, it will likely arrive at the second receiver R2 first due to that receiver being closer than others. Other receivers will likely receive the perturbation from the same point 736 successively later due to the geometry of the receivers with respect to the point 736. The differences in the arrival times can also be affected by variations in the velocity of sound in the medium. Whatever the cause may be, the arrival times

need to compensated for each of the receivers of interest from which the signals (or digitized data therefrom) are combined. One technique of performing such compensation is described below in greater detail.

FIG. 23B shows example traces **760** associated with transmission from an i-th transmitter Tx(i). Similarly, each of the sampled traces **760** can be sampled between a "Start" time and a "Stop" time while being referenced to a time reference. The time reference may or may not be the same as the master time reference described above in reference to FIG. 23A. One can see that because of the proximity of the example point **736** to the second receiver R2, the perturbation signal will likely reach R2 first, followed by successively later arrivals to other receivers spaced from R2. The arrival times within the traces **760** can also be compensated for by the method described below.

From FIGS. 23A and 23B, one can see that signal traces (raw or digitized) from different "sets" associated with different transmitters can be combined. So, if one wants to analyze the return signals from receivers that are offset by one unit from their respective transmitters, the R2 trace from the traces **750** can be combined with the trace (i+1) from the traces **760** (e.g., if i=3, then get trace from R2 and/or R4). Combining signals in such a manner allows enhancement of the perturbation signal while generally maintaining a similar "perspective" with respect to the transmitters.

FIGS. 24 and 25 now show examples of specific possible combinations of offset-one and offset-two data associated with the example operating configuration of FIG. 22. For the purpose of describing the combinations of traces associated with different transmitters, the traces are depicted in a simplified manner as to have already been digitized. Thus, the spikes in the traces represent the digitized values of the sampled perturbation signals (of FIGS. 23A and B).

FIGS. 24A-F show sampled data traces from the receivers associated with each of the six example transmitters. FIGS. 25A-F show the same sampled data traces.

FIGS. 24A-F and G show possible combinations of offset-one data, and FIGS. 25A-F and G show possible combinations of offset-two data. Thus, one can see that the same set of data traces from the receivers associated with each of the transmitters can be used for different offset combinations. Furthermore, offset-three, four, or any number can be achieved in a similar manner as that described in reference to FIGS. 24 and 25.

As shown in FIG. 24A where transmitter Tx1 is used, R2 is the offset-one receiver. As shown in FIG. 24B where transmitter Tx2 is used, R1 and R3 are offset-one receivers; thus, data from either or both receivers can be used. Similar offset-one receivers corresponding to other transmitters are shown in FIGS. 24C to 24F.

FIG. 24G shows a combined data **772** that can result from combination of data **770a-f** for offset-one receivers. If the data are combined properly, the combined data **772** can include an enhanced peak **774** that corresponds to a feature of interest. A method for performing such combination is described below in greater detail.

FIGS. 25A-F and G show possible combinations of offset-two data. As shown in FIG. 25A where transmitter Tx1 is used, R3 is the offset-two receiver. As shown in FIG. 25B where transmitter Tx2 is used, R4 is the offset-two receiver. As shown in FIG. 25C where transmitter Tx3 is used, R1 and R5 are offset-two receivers; thus, data from either or both receivers can be used. Similar offset-two receivers corresponding to other transmitters are shown in FIGS. 25D to 25F.

FIG. 25G shows a combined data **782** that can result from combination of data **780a-f** for offset-two receivers. If the

data are combined properly, the combined data **782** can include an enhanced peak **784** that corresponds to a feature of interest. A method for performing such combination is described below in greater detail.

One can see that other receiver offset (three, four, etc.) data can also be combined in a similar manner. Thus, it will be understood that the example description of the offset-one and offset-two configurations is in no way intended to limit the scope of the present teachings.

FIGS. 26-33 now show how signals from different receivers can be combined so as to yield an enhanced signal of interest. It will be understood that the different receivers can be offset receivers, or simply part of multiple receivers.

FIG. 26 shows that a given receiver **792** can output an example signal **796** having fine perturbations **798** as described above in reference to FIGS. 16 and 17. Such a receiver signal **796** can result from return signals **802** impinging on the receiver **792** from a plurality of directions, including a direction substantially directly in front of it. An imaginary line **790** that extends substantially directly front of the receiver is shown in FIG. 26. For the purpose of description, the line **790** is shown to intersect a layer **794**. Although the line **790** and the layer **794** are depicted as being perpendicular, it will be understood that such orientation is not a requirement. A line may be oriented at an angle with respect to the layer. Furthermore, a layer does not need to have a planar shape—it can be curved and form a portion of a shell-like structure about the receiver.

In one embodiment, receiver signals are combined so as to enhance or "focus" on perturbation features positioned generally along the line **790** and within the layer **794**. Such "focused" combination of signals from a plurality of receivers can be thought of as a scanline associated with the receiver **792**. A plurality of such scanlines associated with a plurality of receivers can then form an image along the scanlines.

FIG. 27 shows that a plurality of example scanlines **812a-c** associated with a plurality of receivers **810a-c** can intersect with an example layer **814**. It will be understood that areas defined by such intersections are not necessarily equivalent to a "pixel." In some applications, the size of a pixel essentially places a limit on the resolution of the image generated therefrom, whether or not the detector is capable of better resolution.

In FIG. 27, an example area **818** is defined as an intersection area defined by the scanline **812b** and the layer **814**. In one embodiment, such an area defines a window (or depth-of-field of the scanline) in which a focus is performed. In one embodiment, if the area is not divided up any more, then that area can be considered to be a pixel for the purpose of imaging.

In one embodiment, the size of the focus area defined in the foregoing manner does not need to be fixed. As described below in greater detail, the layer **814** can be initially selected to be relatively large. Once a "coarse focus" is achieved for such a layer, that layer can be split into thinner layers. Then, the scanline(s) can be "fine focused" if desired and/or able to. Thus, as shown in FIG. 27, the layer **814** can be split into thinner layers such as an example layer **816**, and a focus area **820** would be associated with that relatively thinner layer.

FIGS. 28 to 30 now show by example how scanlines associated with three example receivers can be brought into focus at different layers. For the purpose of description, an example array of three receivers **810a-c** are shown in FIGS. 28A, 29A, and 30A. Associated with the receivers **810a-c** are imaginary lines **812a-c** that extend therefrom respectively. For the purpose of description, the lines **812a-c** are divided into three example layers **822a-c**. Also for the purpose of description, a

first feature of interest **824** is shown to be located generally in an area defined by the line **812a** and the layer **822b**. A second feature of interest **826** is shown to be located generally in an area defined by the line **812b** and the layer **822a**. A third feature of interest **828** is shown to be located generally in an area defined by the line **812c** and the layer **822c**. For the purpose of showing how different features of interest can be shifted in sampling time, the three features of interest are depicted as triangle **824**, circle **826**, and square **828**.

FIGS. 28B, 29B, and 30B are also common, showing that data traces **830a-c** associated with their respective receivers **810a-c** “sees” the three example features of interest **824**, **826**, and **828** at relatively different times. For example, the triangle **824** is generally in front of and closest to the receiver **810a**. Consequently, as the data trace **830a** associated with the receiver **810a** shows, the receiver **810a** will likely receive a return signal from the triangle **824** first, followed by the receiver **810b**, which in turn is followed by the receiver **810c**. Similarly, the circle **826** is generally in front of and closest to the receiver **810b**. Consequently, as the data trace **830b** shows, the receiver **810b** will likely receive a return signal from the circle **826** first, and the receivers **810a** and **810c** after that.

As shown in FIGS. 28A, 29A, and 30A, the receivers **810a-c** are depicted as being arranged in an ordered array. It will be understood that such a depiction is only for the purpose of describing the concept of relative arrival times of return signals to the different receivers, and how such signals can be combined to form a focused scanline. In particular, it will be understood that although the example receivers **810a-c** are shown in sequence, they do not necessarily need to be as such physically. For example, different receiver-offset data can be combined as described above; and in such situations, the receivers whose signals are being combined may not be next to or even relatively close to each other. Thus, the arrangement of the receivers **810a-c** should be considered to represent a logical arrangement for the purpose of description.

FIG. 28C shows an example focused layer **838a** for a scanline **834** associated with the receiver **810a**. Depicted along with the scanline **834** are relative peak heights **836** associated with the combined return signals from the three features **824**, **826**, and **828** when the scanline is in focus. Relative shifting of return signal traces to achieve the focus is shown as a set **832** of shifted traces. It will be noted that one does not need to know how much to shift one trace relative to another trace beforehand to achieve a focus. A method for determining a focused state from different combinations of shifting is described below in greater detail. For the purpose of describing the result of such focusing for a given scanline in reference to FIGS. 28-30, the scanlines are depicted as being brought into focus.

Similarly, FIG. 28D shows an example focused layer **838b** for the scanline **834** associated with the receiver **810a**. Depicted along with the scanline **834** are relative peak heights **836** associated with the combined return signals from the three features **824**, **826**, and **828** when the scanline is in focus. Relative shifting of return signal traces to achieve the focus is shown as a set **840** of shifted traces.

Similarly, FIG. 28E shows an example focused layer **838c** for the scanline **834** associated with the receiver **810a**. Depicted along with the scanline **834** are relative peak heights **836** associated with the combined return signals from the three features **824**, **826**, and **828** when the scanline is in focus. Relative shifting of return signal traces to achieve the focus is shown as a set **844** of shifted traces.

In FIG. 28D, one can see that the focused layer **838b** results in an enhance peak **842** corresponding to the aligning (by proper shifting of the data traces) of the triangle **824**. Such enhanced peaks can be utilized to determine whether a scanline is in focus in a given layer. Such determination is described below in greater detail.

Also note that for the line **812a** associated with the receiver **810a**, the first and third layers **822a** and **822c** do not have any features. Thus, an image resulting from a properly focused scanline should not show features in those two layers **822a** and **822c**. In one embodiment, such result can be achieved by making a threshold cut on the peak(s) in a given focused layer so that peaks below that threshold are not processed for image formation. For example, if one was to set the threshold so as to accept the enhanced peak **842** but reject lower peaks, the first and third focused layers **838a** and **838c** can form focus areas having substantially null images.

FIG. 29C shows an example focused layer **848a** for a scanline associated with the receiver **810b**. Depicted along with the scanline are relative peak heights associated with the combined return signals from the three features **824**, **826**, and **828** when the scanline is in focus. Relative shifting of return signal traces to achieve the focus is shown as a set **846** of shifted traces.

Similarly, FIG. 29D shows an example focused layer **848b** for the scanline associated with the receiver **810b**. Depicted along with the scanline are relative peak heights associated with the combined return signals from the three features **824**, **826**, and **828** when the scanline is in focus. Relative shifting of return signal traces to achieve the focus is shown as a set **852** of shifted traces.

Similarly, FIG. 29E shows an example focused layer **848c** for the scanline associated with the receiver **810b**. Depicted along with the scanline are relative peak heights associated with the combined return signals from the three features **824**, **826**, and **828** when the scanline is in focus. Relative shifting of return signal traces to achieve the focus is shown as a set **854** of shifted traces.

In FIG. 29C, one can see that the focused layer **848a** results in an enhanced peak **850** corresponding to the aligning (by proper shifting of the data traces) of the triangle **826**. Such an enhanced peak can be used to form an image for the area associated with the line **812b** and the layer **848a**.

FIG. 30C shows an example focused layer **858a** for a scanline associated with the receiver **810c**. Depicted along with the scanline are relative peak heights associated with the combined return signals from the three features **824**, **826**, and **828** when the scanline is in focus. Relative shifting of return signal traces to achieve the focus is shown as a set **856** of shifted traces.

Similarly, FIG. 30D shows an example focused layer **858b** for the scanline associated with the receiver **810c**. Depicted along with the scanline are relative peak heights associated with the combined return signals from the three features **824**, **826**, and **828** when the scanline is in focus. Relative shifting of return signal traces to achieve the focus is shown as a set **862** of shifted traces.

Similarly, FIG. 30E shows an example focused layer **858c** for the scanline associated with the receiver **810c**. Depicted along with the scanline are relative peak heights associated with the combined return signals from the three features **824**, **826**, and **828** when the scanline is in focus. Relative shifting of return signal traces to achieve the focus is shown as a set **864** of shifted traces.

In FIG. 30E, one can see that the focused layer **858c** results in an enhanced peak **860** corresponding to the aligning (by proper shifting of the data traces) of the square **826**. Such an

enhanced peak can be used to form an image for the area associated with the line 812c and the layer 858c.

In one embodiment, a layer closest to a given receiver is focused first, followed by successive layers therefrom. Focusing of a given layer allows determination of propagation time within that layer, since the amount of shifting of various data traces depends on how much differences there are in the propagation times. Thus, a given layer is brought into focus when the proper amount of shifting is applied (i.e., when the proper propagation time is determined for that layer).

In one embodiment, the foregoing focusing process and/or the focus results therefrom can be implemented with physical movements of one or more transducer elements. For example, arrays having movable elements similar to that of adaptive optics can be adjusted to either aid the focusing process, or to re-position the elements so that subsequent focusing process can be achieved more efficiently. In one specific example, suppose that a focused section of a scanline is achieved when data traces from one or more receivers are shifted so as to be near their limits. In such cases, the corresponding receivers may be moved so as to introduce changes in propagation times thereto, so that likely "focused" sections of the corresponding data traces are now located more centrally, thereby providing more "working" room in the shifting of data traces.

By focusing on the closest layer, the propagation time for that layer is determined. Focusing of the next layer can then be facilitated by the knowledge of the first layer. This building of propagation time information can build successively outward away from the receiver.

It will be understood that the shifting of data traces described for the purpose of combining those data traces refer to shifting in time. In one embodiment where each data trace includes a series of digital representation of samplings, each sampling has a time associated with it. Thus, time-shifting can be in the form of shifting data trace based on such "time stamp" of the samplings. Based on the foregoing, a "time-shift combination" operation includes shifting of time or phase associated with portions of a plurality of data traces with respect to each other. For example, if a scanline is being focused at a given layer, temporal ranges of data traces being combined can be identified (for example, by an initial estimation based on geometry). Then, digital data within those ranges can be shifted with respect to each other and combined to yield a quality value associated with that combination.

FIGS. 31A-C show such a successive layer characterization method. In FIG. 31A, an arrow 872 directed away from a receiver indicates the order of layer characterization. Also in FIG. 31A, an example layer 866 is shown. If that layer is to be split for finer focusing, such as layers 868a and 868b in FIG. 31B, characterization of those sub-layers can be characterized successively beginning from the sub-layer closest to the receiver (as indicated by an arrow 874). Similarly, each of the sub-layers 868 can be split further into layers 870a-b and 870c-d. Again, such layers can be characterized successively beginning from the one closest to the receiver (as indicated by an arrow 876).

It will be understood that the foregoing successive layer characterization (beginning with the closest layer to the receive) is just one example of focusing on the plurality of layers. As described herein, focusing on a given layer does not necessarily depend on the knowledge of another layer. Thus, focusing can begin at any layer in the medium without departing from the scope of the present teachings.

FIGS. 32-33 now show how a scanline can be focused at a given layer—that is, how signal traces from different receivers can be combined so as to optimally enhance perturbation features of interest. For the purpose of describing the focusing

technique, "velocity" (generally inversely proportional to time) is used to characterize the propagation time within a given layer. It should be noted that in the focusing technique of FIG. 32-33, a prior knowledge of velocity is not necessary.

5 FIG. 32 shows a process 880 for determining focused scanlines for one or more receivers at different layers. In one embodiment, the process 880 further includes finer-focusing capability that splits a given layer if that split provides an improved scanline focus quality. The process 880 in general includes a process block 882 where input parameters are obtained. Some of the input parameters are described in a more specific process in reference to FIG. 33.

10 The process 880 then loops through the receivers (end loop 914). In a process block 886, the process 880 determines the position of a scanline corresponding to the current receiver. For the current receiver, the process 880 loops through each of the Z layers (end loop 912). In one embodiment, the layers are successively looped through from layer one to layer Z, with layer one being the closest to the receiver.

15 20 For the current receiver and the current layer, the process 880 in a process block 890 determines a velocity value that results in the best degree of focus for the current scanline in the current layer. Various methods of determining the degree of focus selecting the "best" therefrom are described below in greater detail. As previously described, a prior knowledge of velocity value is not necessary. However, providing a likely range of velocity values may result in a more efficient combinatoric computation for combining and determining the degree of focus.

25 30 The process 880 in a process block 890 then updates the velocity data corresponding to the current scanline and the layer. Such data can be stored as a table, or any manner that allows retrieval for later use.

35 In one embodiment, the current layer is initially split into sub-layers in a process block 894, and focusing is performed in each of the newly created sub-layers in a sub-layer loop 896 (end loop 900). Each of these sub-layers may be further split, and each of those newly created layers may undergo similar loop. This successive splitting process may continue further. 40 Thus, for the purpose of description, the sub-layer loop 896 is depicted as a module that can be accessed whenever a set of sub-layers are looped through.

45 50 Within the sub-layer loop 896, the process 880 in a process block 898 determines a velocity value that results in the best degree of focus for the current sub-layer. Whether that velocity value will replace the existing velocity value for the area overlapping the current sub-layer depends on whether the current sub-layer focus is an improvement. In one embodiment, such determination can be made on a sub-layer by sub-layer basis, or collectively for the set of sub-layers. As an example, an average of the degrees of focus for the sub-layers can be compared to the degree of focus for the parent layer. For the purpose of description, the process 880 is shown to determine if the degree of focus has improved collectively by the split in a process block 902.

55 Once such determination is made, the process 880 in a decision block 904 determines whether the focus has improved by the split. If the answer is "yes," then the process 880 in a process block 906 updates the velocity table for the sub-layers of the current layers. To see if the focus can be made even finer, thereby improving the resolution, each of the current sub-layers are further split in a process block 908, and focusing is performed on each of the newly created sub-layers by invoking the sub-layer loop 896. If the answer in the decision block 904 is "no," then the process 880 removes the previous split in a process block 910, since the finer "focus" did not yield a better result.

FIG. 33 now shows a more specific example process 920 of how the process 880 of FIG. 32 can be implemented. For the purpose of simplicity, the process 920 is described for one given receiver. But as shown in FIG. 32, such a process can be looped over a plurality of receivers.

The process 920 in a process block 922 determines the position of a scanline associated with the receiver being analyzed. In a process block 924, a maximum number of sub-layers within a given layer is obtained. In one embodiment, that maximum number places a limit on the extent of splitting for finer focusing. In a process block 926, the process 920 obtains a level of focus quality improvement to trigger additional splitting for finer focusing. In a process block 928, the process 920 obtains a current velocity table for the layers if available and/or desired. In a process block 930, a seedpoint (such as a value representative of a lowest expected velocity) is obtained if available and/or desired. In a process block 932, the process 920 obtains the range and increment of velocity for determining the velocity associated with the best degree of focus.

The process 920 then loops through layers one to Z in a loop 936 (end loop 960). For each current layer, the process 920 loops through the range of velocity values in a loop 936 (end loop 942). For the current velocity value, the process 920 generates a scanline at the current layer in a process block 938. The process 920 then determines a degree of focus of the scanline for the current velocity in the process block 940.

Once the process loop 936 is completed, the process 920 in a process block 944 determines a velocity that results in the best degree of focus for the current layer. In a process block 946, the process 920 splits the current layer into two sub-layers if the current number of sub-layers is less than the selected maximum number of sub-layers (obtained in the process block 924). In a process block 948, the velocity table is updated with the velocity value that gave the best degree of focus for the current layer.

The process 920 then loops through the newly created sub-layers (if any) in the process block 946 in a loop 950 (end loop 954). For each sub-layer, the process 920 in a process block 952 loops through the velocity range and determines a velocity value that results in the best degree of focus for that sub-layer in a manner similar to that of the loop 936. The process 920 then determines if degree of focus associated with the sub-layers is better than that of the parent layer in a process block 956. In one embodiment, the new degree of focus is considered to be better than that of parent layer if it exceeds the level of focus quality improvement obtained in the process block 926.

If the sub-layer degree of focus is better than the parent layer degree of focus, the process 920 in a process block 958 updates the velocity table and splits each of the current sub-layers into two sub-layers. Again, this splitting can be limited by the maximum number of sub-layer as determined in the process block 924. If the sub-layer degree of focus is not better than the parent degree of focus, the process 920 removes the previous split and retains the parent layer level of focus.

In the description herein in respect to FIGS. 26-33, various references are made about focusing, degree of focus, and the like. FIGS. 34A and B now show by example how a focus can be achieved by determining a parameter representative of the best degree of focus. A “focus” associated with an array of signal values can be determined in a variety of ways. For example, some autofocus cameras compare relative contrasts of adjacent or nearby signal values—the reason being that a sharply focused image will have more of a sudden change in

the contrast. A similar method can be applied for determining the degree of focus for a scanline of interest.

In one embodiment, the splitting of layers can provide a substantial advantage in how effectively a given volume can be imaged. As an example, suppose that a volume includes a relatively small group of features of interest localized in a relatively small region. The rest of the volume is substantially homogeneous for the purpose of propagating signals. Such homogeneous portions likely will not need to be split, since the velocity therein is substantially uniform. When the small inhomogeneous region is encountered, it can be split into smaller layers to allow characterization of sub-regions with different velocity values. Thus, one can see that the combining process does not need to waste time attempting to split the homogeneous portion. Moreover, the inhomogeneous region can be characterized better by the splitting method, thereby allowing improved characterization of the volume.

FIG. 34A shows the shifted data trace set 840 corresponding to “in focus” configuration as described above in reference to FIG. 28D. FIG. 34A further shows one of a number of possible ways of determining the degree of focus for the trace combination set 840. In one embodiment, a running average of the combined scanline is obtained for a selected window. In one embodiment, such a window may overlap the focus layer 838b and extend beyond. In one embodiment, the window may be defined as temporally substantially similar to the boundaries corresponding to the focus layer 838b.

In one embodiment, the running averages are formed by a plurality of partially overlapping averaging intervals 970. Average values 972 associated with the intervals 970 are depicted at the approximate centers of the intervals 970.

FIG. 34B shows a shifted data trace set 980 corresponding to “almost in focus” configuration. In particular, the combination 980 has the second trace (990 in FIG. 34B) not shifted as much as that of FIG. 34A. Average values 982 associated with the running average intervals are also shown.

In one embodiment, a best degree of focus can be determined by looking for the greatest change in the running average value. Thus in the example scanlines shown in FIGS. 34A and B, a change in average denoted as 974 is has the greatest slope (i.e., the greatest “contrast”) within the window. The data trace combination 840 corresponds to the greatest slope 974, and thus represents the “in focus” scanline having the best degree of focus value (in this example, the greatest slope).

In another embodiment, a best degree of focus can be determined by looking for the greatest sum of average values within the window. In FIGS. 34A and B, one can see that the average values 972 add up to a greater value than that of the average values 982. Thus, the data trace combination 840 can be said to be the “in focus” scanline having the best degree of focus value (in this example, the sum of average values).

One can see that there are many other ways of determining the best degree of focus. Thus, it will be understood that the two examples described above in reference to FIGS. 34A and B are not to be construed as limiting the scope of the present teachings. Furthermore, “quality value” can represent the various degrees of focus described herein, and “best quality value” can represent the corresponding “best degree of focus.” It will be understood that the term “best” does not necessarily mean a value having the largest value. It can mean a value having the smallest value, or any value that represents a particular combination having the desired property for the purpose of assigning to a scanline.

FIGS. 35A and B now show block diagrams of one embodiment of a signal processing assembly 1100 that can perform various functions described herein (such as obtain-

ing data traces from receivers, digitally sampling, and combining the digitally sampled data). As shown in FIG. 35A, one embodiment of the assembly **1100** includes a plurality of data channels **1104** that are input into a data combiner **1106**. Each data channel **1104** forms a stream of digital data corresponding to data traces from one or more receivers in a manner described below in greater detail. Thus in one embodiment, such digital data represents digital echo signals having amplitudes and time information of samplings of the data traces.

As shown in FIG. 35A, such digital data from the data channels **1104** are combined by a data combiner **1106**. In one embodiment, the data combiner **1106** combines the digital data according to the relative orientation of the receivers with respect to transmitters. For example, data corresponding to offset-one receivers can be combined as one set of data. In one embodiment, such combining of data is performed by parallel processing (as depicted in FIG. 35A) so as to allow timely processing of relatively large amount of data.

In one embodiment, each stream of data in the channel **1104** is associated with a receiver and a transmitter. Thus, focus information can be associated with such receiver and/or transmitter can be provided to the channel **1104** by a focus parameter database **1122**. For example, for pixel imaging, the focus information can include the transmitter and receiver alignment sets. For focusing on a layer along a scanline, the focus information can include default velocity information for the receivers.

Thus in one embodiment, an output from the data combiner **1106** represents group(s) of data corresponding to different receiver-transmitter combinations. As shown in FIG. 35A, such combined data can form a “page” of data, and such pages of data can be further combined by a page combiner **1108**. For example, pixel intensity as determined by selected groups of transmitter-receiver combinations (pages) can be further combined to enhance the real signal from that pixel, by using the transmitter-pixel and pixel-receiver geometries. In another example, pages of data can be combined with respect to a scanline for a receiver at a given layer, such that each combination yields a degree of focus or a quality value. As described above, a “best” degree of focus or quality value can be determined in a number of ways to select a “best” scanline for the receiver.

As shown in FIG. 35A, an output from the page combiner **1108** can be stored in a page memory **1110**. Such stored page combinations can be refined further as shown. For example, the finer focusing by layer-splitting described above can be facilitated by such a feature.

In one embodiment, the page memory **1110** can include a plurality of “final” pages of data that can be used for imaging. As shown in FIG. 35A, such pages of data can be processed further to clean up the data and/or map to a display representation in a re-map/filter block **1112**. Output from the block **1112** can be built into a frame of image in a frame buffer **1114**, and be displayed via a display **1116**.

FIG. 35B now shows one embodiment of each of the data channel **1104** described above in reference to FIG. 35A. The data channel **1104** is shown to include an optional multiplexer **1132** that receives as inputs **1130** analog data traces from a plurality of receivers (not shown). In one embodiment, the multiplexer is not used, and data trace from one receiver is input into one data channel.

As shown in FIG. 35B, the multiplexer output (or signal from the receiver) can be amplified by a pre-amp **1134** and have its temporal gain corrected by a TGC **1136**. The output from the TGC **1136** is shown to be digitally sampled by an ADC **1138** (analog-digital converter). In one embodiment,

the ADC **1138** is a 12- or 16-bit amplitude ADC that samples the amplitude of the data trace at a sampling frequency.

As shown in FIG. 35B, the output from the ADC **1140** can be cleaned up and/or formatted for subsequent processing by an optional correlator/filter **1140**. The output from the correlator/filter **1140** is input into a data memory **1142** for combining with the focus information from a focus database **1144** as described above in reference to FIG. 35A. The output from the data memory **1142** is then sent to the data combiner (**1106** in FIG. 35A).

One can see that foregoing example signal and data processing, such as combining of different pages of data to determine the best scanline for a given receiver, can involve a substantially large amount of computation. Timely computation of such a task can be achieved, in one embodiment, by parallel processing.

One can also reduce the amount of computation in combining of data by limiting the combinations to a selected window in time. For example, suppose each digital echo data has N samples so as to represent a sampling duration of T . As described above, one way to form an image of a scanline is to focus onto a layer that intersects with the scanline. Such a layer with a given thickness is positioned from the receiver in a known manner. Thus one can estimate the approximate time values associated with the layer based on its relative position and its thickness by knowing the average propagation velocity of the echo signal in the medium. So to image the scanline for that layer, one can limit the digital echo data to a range that corresponds to the layer thickness.

FIGS. 36A and B now show an example image obtained using some of the imaging methods described herein. FIG. 36A shows a black-and-white photograph of the image. FIG. 36B shows a negative image of the photograph of FIG. 36A. A sectional view of a plurality of wires **1200** is formed by imaging a slice through a medium **1202** where the wires are located. Each wire has a diameter (denoted as **1204**) of approximately 100 micrometers, and a spacing (denoted as **1206**) between (edge-to-edge) two closest adjacent wires is approximately 100 micrometers. The medium **1202** is water contained in a volume of approximately 350 cm^3 , and the wires are located approximately 6.7 cm from an array of receivers (not shown).

To obtain such an image, **32** receivers were used to receive echo signals that resulted from sequenced transmission energy from **32** transmitters. The transmission energy was transmitted at approximately 3.5 MHz, and the echo signals detected by the receivers were sampled at a rate of approximately 20 MHz.

One can readily see from FIGS. 36A and B that the resulting high quality and contrast image displays a spatial resolution that appears to be better than 100 micrometers. For the example transmitted 3.5 MHz signal, a corresponding wavelength in water is approximately 440 micrometers (for an average velocity of 1540 m/s). Thus, one can see that resolving of a 100 micrometers feature at the transmitted energy frequency of 3.5 MHz is equivalent to a resolution being better than quarter of the operating wavelength.

In terms of Nyquist sampling criteria, the example 3.5 MHz signal would require sampling at a rate of approximately 7 MHz (twice the signal frequency) or higher for conventional devices. In a similar token, measurement of an example feature size of 100 micrometers would require a sampling rate of approximately 30.8 MHz (twice the frequency that can be assigned to a 100-micrometer feature size—i.e., $1540 \text{ [m/s]}/100 \text{ [micrometers]} = 15.4 \text{ MHz}$) for conventional devices. Thus, one can see that sampling at multiple receivers and combining data therefrom can yield a

high-quality result even if the sampling rate (example, 20 MHz) is less than the conventional Nyquist limit (example, 30.8 MHz).

From the description of the example image and the methods used herein, it is apparent that one can obtain a spatial resolution that is less than the wavelength associated with an operating transmission energy. Intrinsic resolution of a detector is often expressed in terms of λ/D , a ratio of the operating wavelength λ and the effective aperture size D of the detector. A constant factor associated with such a ratio can vary depending on the configuration of a particular detector. For the purpose of description herein, it will be assumed that the intrinsic angular resolution is represented as $\theta = \lambda/D$.

One can reduce the value of θ (i.e., increase of "better" the resolution) by either reducing the wavelength and/or increasing the detector size D . The effective size D of the detector can be increased either by increasing the individual detector size, or by forming an array whose overall size can be substantially larger than that of each detector. Such methods have been used in some fields. In the field of ultrasound imaging, Applicant believes that currently, the image quality and resolution as disclosed herein has not been achieved using conventional systems and methods. For example, one embodiment of the imaging system and method yields an angular resolution that is equivalent to using a wavelength that is less than a quarter of the operating wavelength for a given detector size D . That is, the resolution is better than $\theta = (0.25)\lambda/D$ in one embodiment.

From the description herein it is also apparent that the sampling frequency can be less than the frequencies associated with perturbation features that "ride" on the "carrier-wave" echo of the transmission energy. One way to characterize such performance is by way of Nyquist criteria that essentially states that a signal needs to be sampled at a frequency F that is at least twice the frequency of the signal to obtain any useful information. Thus for example, if a signal has a frequency of 1 MHz, it needs to be sampled at 2 MHz or higher.

If the sampling frequency is less than twice the signal frequency, an effect known as "aliasing" occurs, where frequencies above the Nyquist frequency ($F/2$) "fold over" to behave like lower frequencies. As is known, aliased frequency f in the range $F/2$ to F becomes f' that can be expressed as $|f-F|$.

From the description herein, it is apparent that in one embodiment (that produces the example image of FIGS. 36A and B, for example), the sampling frequency can be less than twice the frequency associated with the size feature of interest. For example, the feature size of the wires in FIGS. 36A and B is approximately 100 micrometers, and its corresponding "frequency" can be represented as approximately $(1540 \text{ mls})/(100 \text{ micrometers}) = 15.4 \text{ MHz}$. From the results obtained by sampling at approximately 20 MHz (which is less than twice the frequency corresponding to the feature size), one can see that such relatively small perturbation features can be imaged with excellent quality and resolution.

It should be noted that for the purpose of description, the term "frequency" means the frequency associated with the central peak associated with the signal. Thus, if the signal is a sinusoidal wave, its frequency corresponds to the standard meaning. If the signal is a pulse (e.g., Gaussian shaped), then the frequency corresponds to the central peak of the pulse. If the signal is a perturbation feature having a peak structure, then the frequency corresponds to that peak.

With such example definition of frequency, one can characterize the performance of the present teachings as being able to image an echo signal in terms of spectral frequency

components. If a given echo signal has a maximum intensity value, then the resolvable spectral frequency components above the Nyquist frequency of $F/2$ can include higher frequency components having intensities that are above a predetermined value. Such a predetermined value can be set at different values, such as 50 dB, 40 dB, 30 dB, 20 dB, 10 dB, or 10 dB less than the maximum intensity value the echo signals.

Although the above-disclosed embodiments have shown, described, and pointed out the fundamental novel features of the invention as applied to the above-disclosed embodiments, it should be understood that various omissions, substitutions, and changes in the form of the detail of the devices, systems, and/or methods shown may be made by those skilled in the art without departing from the scope of the invention. Consequently, the scope of the invention should not be limited to the foregoing description, but should be defined by the appended claims.

20 What is claimed is:

1. A method for ultrasonic imaging of an object, the method comprising:

in turn, for each transmitter in a plurality of transmitters, transmitting ultrasound energy from the transmitter into the object such that the ultrasound energy is scattered and detecting the scattered energy at each of a plurality of receivers to obtain signals corresponding to a plurality of transmitter-receiver pairs wherein each transmitter-receiver pair is characterized by a value, N , indicative of a spatial separation between the transmitter and the receiver of the transmitter-receiver pair;

processing the signals by:

preparing a first page by: for each pixel in a plurality of pixels within the object, sampling a plurality of those of the signals corresponding to transmitter-receiver pairs characterized by a first value of N at a first index representing a time delay corresponding to the pixel, transmitter and receiver to yield a first set of sample values corresponding to the pixel the first set of sample values including only sample values from transmitter-receiver pairs having the first value for N ; and combining the values of the first set of sample values to provide first pixel values associated with the first page of data; and

preparing one or more additional pages, each corresponding to a different value for N by: for each pixel in the plurality of pixels, sampling a plurality of those of the signals corresponding to transmitter-receiver pairs characterized by the value of N corresponding to the page at a second index corresponding to the pixel, transmitter and receiver to yield another set of sample values corresponding to the pixel the another set of sample values including only sample values from transmitter-receiver pairs having the value of N corresponding to the additional page; and combining the values of the another sets of sample values to yield pixel values associated with the additional page; and, displaying image data based on at least one of the pages.

2. A method according to claim 1 wherein:

the transmitters are provided in an array of transmitters $Tx(i)$, where i represents a relative positional index that ranges from 1 to M , where M is greater than or equal to 2;

the receivers are provided in an array of receivers $Rx(j)$, where j represents the relative positional index of each of said receivers, positional index j being offset from posi-

tional index i by the value N , where N ranges from zero to N_{max} , where N_{max} is a positive value greater than zero; and,

the method comprises:

storing the first page as a page of signal data generated 5 from energy received at said receivers $Rx(j)$ offset from said transmitters $Tx(i)$ by the first value of N .

3. The method of claim 1 comprising:

creating an image from a single one of said pages; and 10 displaying said image.

4. The method of claim 1 comprising:

creating an image from one of said pages; displaying said image;

combining data from two or more of said pages to yield 15 combined data and creating another image from said combined data;

repeating said creating another image from said combined data and displaying said another image at least once, each repetition comprising combining into said combined data at least one additional page not having been 20 previously combined.

5. The method of claim 1, wherein said pages are iteratively combined in a predetermined order.

6. The method of claim 5, wherein said pages are iteratively combined in a sequential order. 25

7. A method according to claim 1 comprising combining at least two of the pages to provide the image data.

8. A method according to claim 1 comprising determining the first index corresponding to the pixel, transmitter and receiver by combining a first index value corresponding to the 30 pixel and transmitter with a second index value corresponding to the pixel and receiver.

9. A method according to claim 1 wherein: the ultrasound energy has a wavelength λ corresponding to 35 a central peak frequency of said ultrasound energy, the transmitters are arranged in a transducer assembly such that an aperture size D is the maximum distance between any two transmitters in the transducer assembly; and the image has a spatial resolution limit θ representing the minimum resolvable angular separation of two features within the object wherein θ is equal to or better than $\theta = (0.25)\lambda/D$.

10. An ultrasound imaging apparatus comprising: a plurality of ultrasound transmitters and a plurality of ultrasound receivers wherein the transmitters are 45 arranged to permit ultrasound energy to be transmitted from the transmitters into an object such that the ultrasound energy is scattered and the receivers are arranged to detect the scattered energy;

a processor configured to process signals from the receivers to yield image data; and, 50

a display for displaying the image data;

wherein the apparatus is configured to, in turn, for each one of a plurality of the transmitters, cause the transmitter to transmit ultrasound energy into the object and to obtain at the receivers signals corresponding to a plurality of transmitter-receiver pairs wherein each transmitter-receiver pair is characterized by a value, N , indicative of a spatial separation between the transmitter and the receiver of the transmitter-receiver pair; and

wherein the processor is configured to process the signals by:

preparing a first page by: for each pixel in a plurality of pixels within the object, sampling a plurality of those of the signals corresponding to transmitter-receiver pairs characterized by the first value of N at a first index representing a time delay corresponding to the pixel, transmitter and receiver to yield a first set of sample values corresponding to the pixel; and combining the values of the first set of sample values to provide first pixel values associated with the first page of data the first set of sample values including only sample values from transmitter-receiver pairs having the first value for N ; and preparing one or more additional pages, each corresponding to a different value for N by: for each pixel in the plurality of pixels, sampling a plurality of those of the signals corresponding to transmitter-receiver pairs characterized by a value of N corresponding to the page at a second index representing a time delay corresponding to the pixel, transmitter and receiver to yield another set of sample values corresponding to the pixel the another set of sample values including only sample values from transmitter-receiver pairs having the value of N corresponding to the additional page; and combining the values of the another sets of sample values to yield pixel values associated with the additional page.

11. Apparatus according to claim 10 wherein:

the ultrasound energy has a wavelength λ corresponding to a central peak frequency of said ultrasound energy, the transmitters are arranged in a transducer assembly such that an aperture size D is the maximum distance between any two transmitters in the transducer assembly; and the image has a spatial resolution limit θ representing the minimum resolvable angular separation of two features within the object, wherein θ is equal to or better than $\theta = (0.25)\lambda/D$.

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专利名称(译)	用于改进的超声成像的系统和方法		
公开(公告)号	US7850611	公开(公告)日	2010-12-14
申请号	US10/945459	申请日	2004-09-20
[标]申请(专利权)人(译)	DAVIES TIMOTHY J EVANS RICHARD		
申请(专利权)人(译)	DAVIES TIMOTHY J EVANS RICHARD		
当前申请(专利权)人(译)	锐珂医疗 , INC.		
[标]发明人	DAVIES TIMOTHY J EVANS RICHARD		
发明人	DAVIES, TIMOTHY J. EVANS, RICHARD		
IPC分类号	A61B8/00		
CPC分类号	G01S7/52028 G01S7/52046 G01S15/8918 G01S7/52003 G01S7/52036 G01S15/8927 A61B8/4483		
其他公开文献	US20060064015A1		
外部链接	Espacenet USPTO		

摘要(译)

公开了用于改善由来自接收器阵列的信号形成的图像的分辨率和质量的系统和方法。多个接收器引入到达时间的变化，其可以小于操作信号的周期，并且还小于与采样操作相关联的周期。因此，多个接收器允许对反射信号的精细特征进行采样，这些特征将被认为超出与操作信号相关联的分辨率。使用多个接收器还提供了有效的采样率，该采样率大于单个接收器的采样率。使用多个发射器可以获得类似的优点。这些有利特征可用于在诸如超声成像的应用中获得介质中的对象的高分辨率图像。

