



US010345444B2

(12) **United States Patent**
Olsson

(10) **Patent No.:** **US 10,345,444 B2**
(45) **Date of Patent:** **Jul. 9, 2019**

(54) **ULTRASONIC DIAGNOSTIC IMAGING SYSTEM WITH SPATIAL COMPOUNDING OF TRAPEZOIDAL SECTOR**

(71) Applicant: **KONINKLIJKE PHILIPS N.V.**,
Eindhoven (NL)

(72) Inventor: **Lars Jonas Olsson**, Eindhoven (NL)

(73) Assignee: **Koninklijke Philips N.V.**, Eindhoven
(NL)

(*) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 343 days.

(21) Appl. No.: **14/778,292**

(22) PCT Filed: **Apr. 24, 2014**

(86) PCT No.: **PCT/IB2014/060079**

§ 371 (c)(1),

(2) Date: **Sep. 18, 2015**

(87) PCT Pub. No.: **WO2014/155265**

PCT Pub. Date: **Oct. 2, 2014**

(65) **Prior Publication Data**

US 2016/0282467 A1 Sep. 29, 2016

Related U.S. Application Data

(60) Provisional application No. 61/804,783, filed on Mar. 25, 2013.

(51) **Int. Cl.**
G01S 15/89 (2006.01)
G01S 7/52 (2006.01)
(Continued)

(52) **U.S. Cl.**
CPC **G01S 15/8995** (2013.01); **A61B 8/14**
(2013.01); **A61B 8/4444** (2013.01);
(Continued)

(58) **Field of Classification Search**

CPC G01S 15/8918; G01S 15/8995; G01S 15/8925; G01S 7/52085; A61B 8/488;
(Continued)

(56) **References Cited**

U.S. PATENT DOCUMENTS

4,159,462 A 6/1979 Rocha et al.
4,245,250 A * 1/1981 Tiemann G01S 7/52044
342/185

(Continued)

FOREIGN PATENT DOCUMENTS

EP 1906207 A1 4/2008
JP 2004154567 A 6/2004
WO 2007099474 A1 9/2007

OTHER PUBLICATIONS

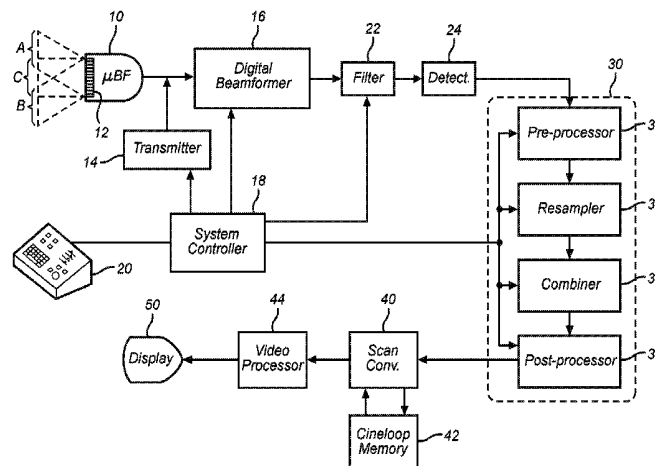
O'Donnell "Optimum Displacement for Compound Image Generation in Medical Ultrasound" IEEE Transactions on Ultrasonics, Ferroelectrics, and Frequency Control, vol. 35, No. 4 Jul. 1988 p. 470-476.

Primary Examiner — Bo Joseph Peng

(57) **ABSTRACT**

An ultrasonic diagnostic imaging system produces spatially compounded trapezoidal sector images by combining component frames acquired from different look directions. A virtual apex scan format is used such that each scanline of a component frame emanates from a different point (E1, En) on the face of an array transducer (12) and is steered at a different scanning angle. For different component frames the scanlines are steered at respectively different angles. In the illustrated example, the scanlines of each component frame are incremented by five degrees relative to the corresponding scanlines in a reference component frame. When the component frames are combined for spatial compounding, the maximum number of component frames are combined over virtually the entire image field.

15 Claims, 6 Drawing Sheets



- (51) **Int. Cl.**
A61B 8/14 (2006.01)
A61B 8/00 (2006.01)
A61B 8/08 (2006.01)
- (52) **U.S. Cl.**
 CPC *A61B 8/4494* (2013.01); *A61B 8/461*
 (2013.01); *A61B 8/488* (2013.01); *A61B*
8/5207 (2013.01); *A61B 8/5238* (2013.01);
G01S 7/52085 (2013.01); *G01S 15/8918*
 (2013.01); *G01S 15/8925* (2013.01)
- (58) **Field of Classification Search**
 CPC A61B 8/461; A61B 8/4494; A61B 8/4444;
 A61B 8/14; A61B 8/5207; A61B 8/5238
 See application file for complete search history.

(56) **References Cited**

U.S. PATENT DOCUMENTS

4,319,489	A	3/1982	Yamaguchi et al.
4,649,327	A	3/1987	Fehr et al.
5,123,415	A	6/1992	Daigle
5,485,842	A	1/1996	Quistgaard
5,860,924	A	1/1999	Quistgaard
6,126,598	A	10/2000	Entrekin et al.
6,210,328	B1	4/2001	Robinson et al.
6,224,552	B1	5/2001	Jago et al.
6,416,477	B1	7/2002	Jago
2006/0293596	A1 *	12/2006	Jago G01S 7/52046 600/437
2009/0016163	A1 *	1/2009	Freeman G01S 7/5208 367/103
2009/0069681	A1	3/2009	Lundberg et al.

* cited by examiner

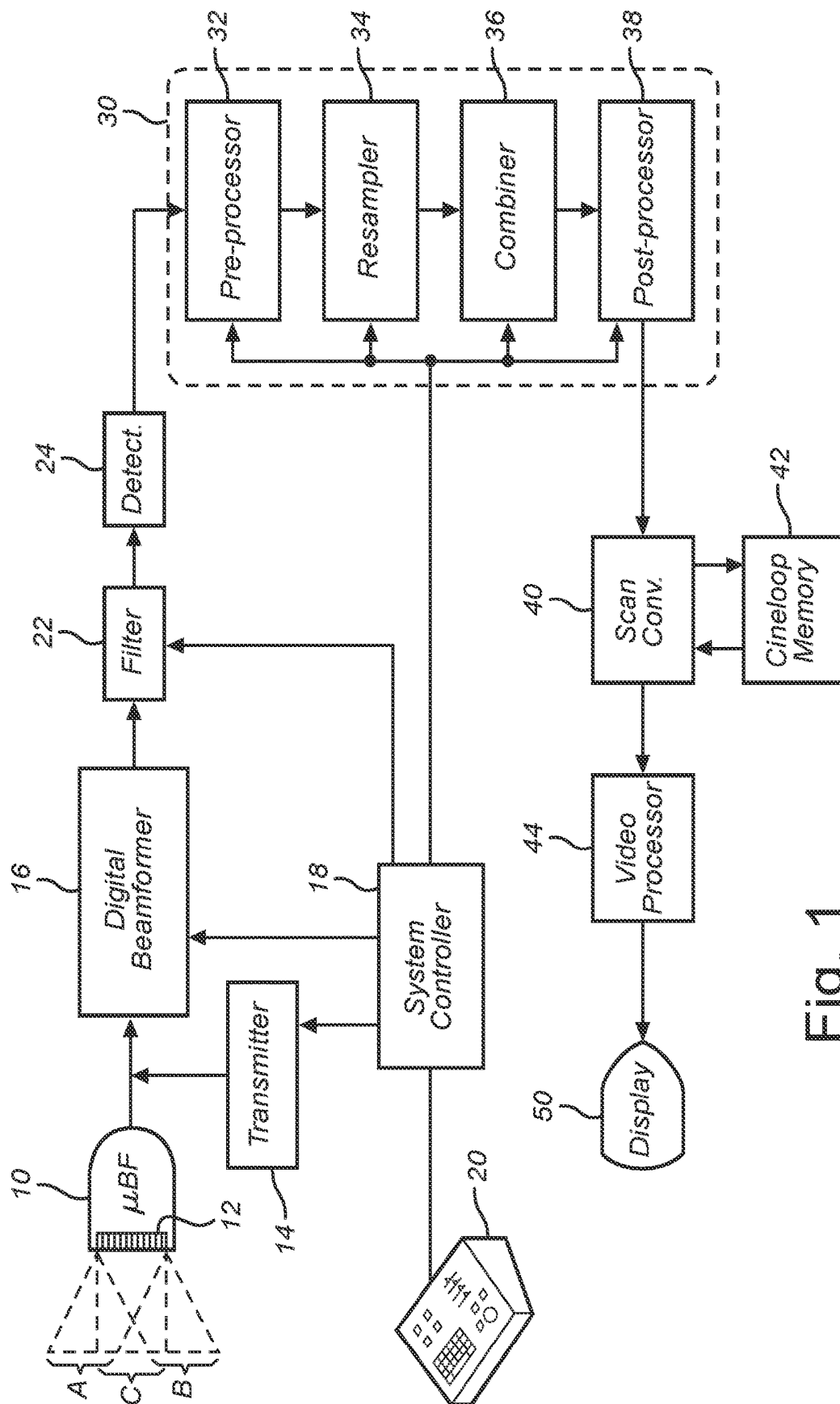


Fig. 1

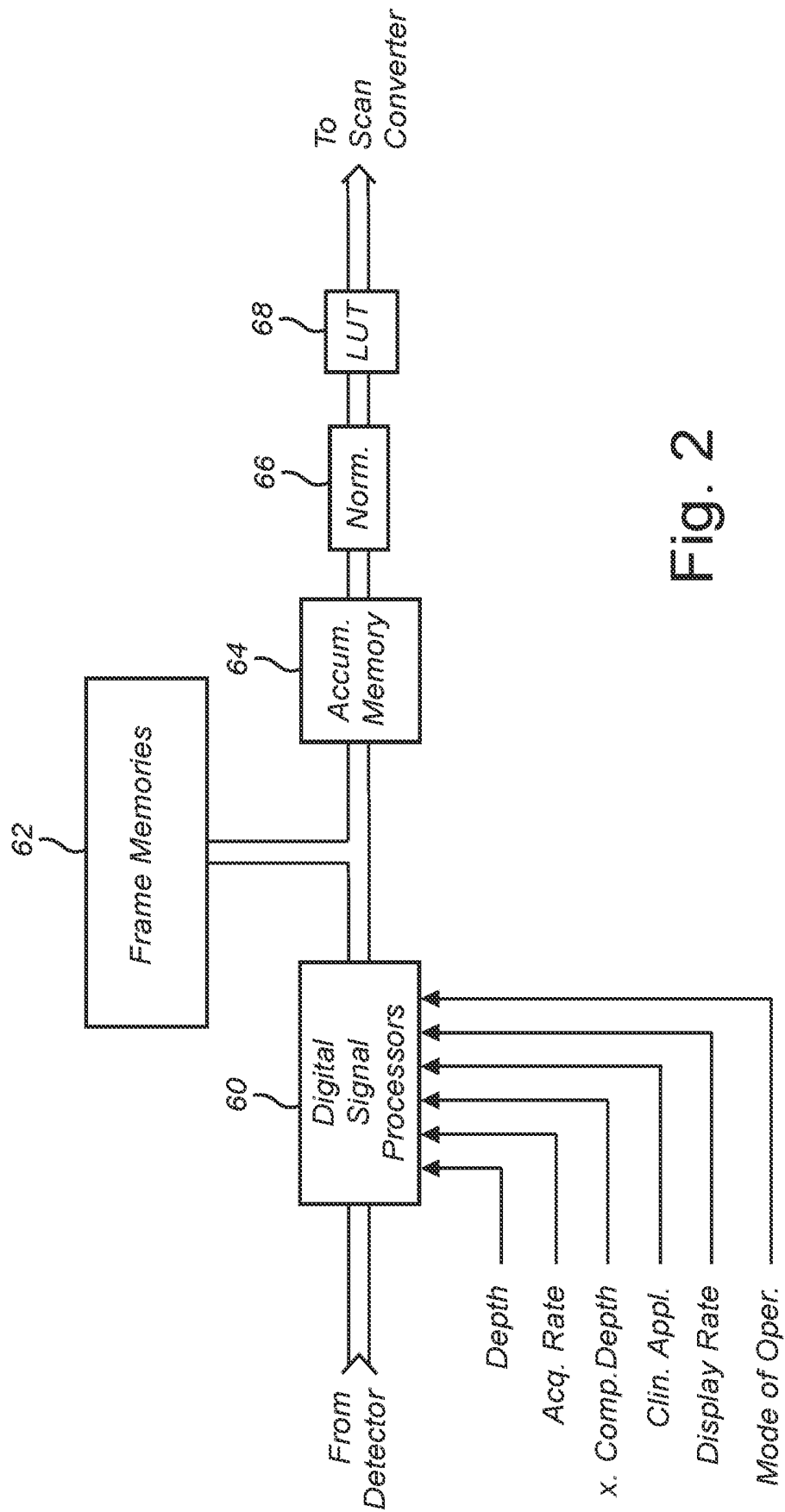
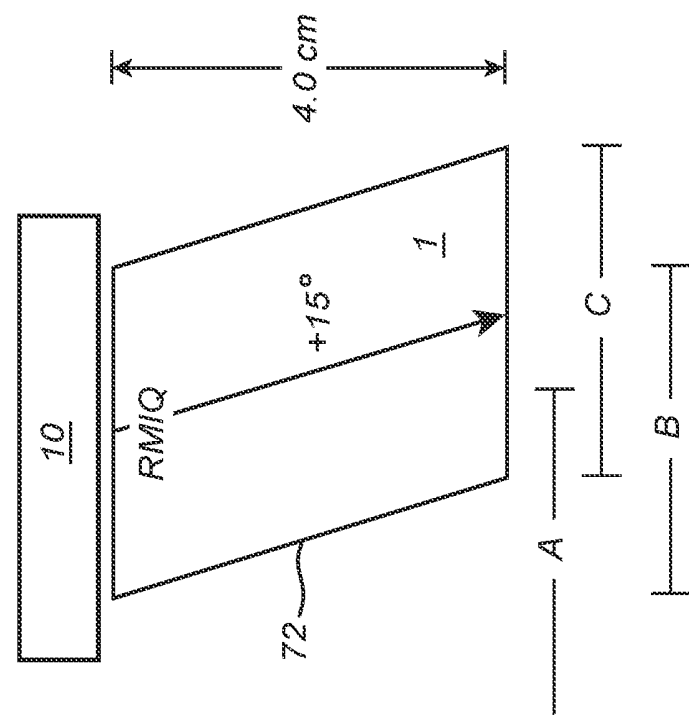
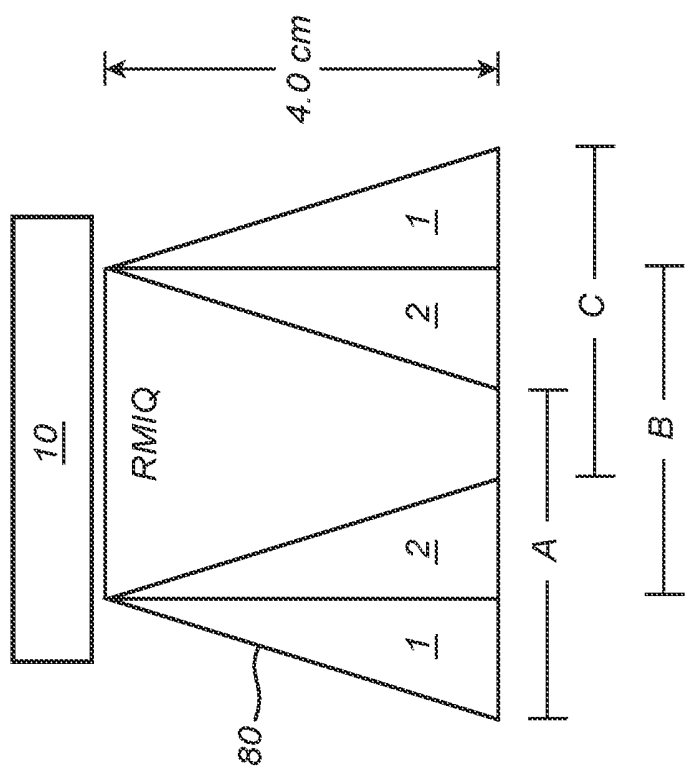


Fig. 2







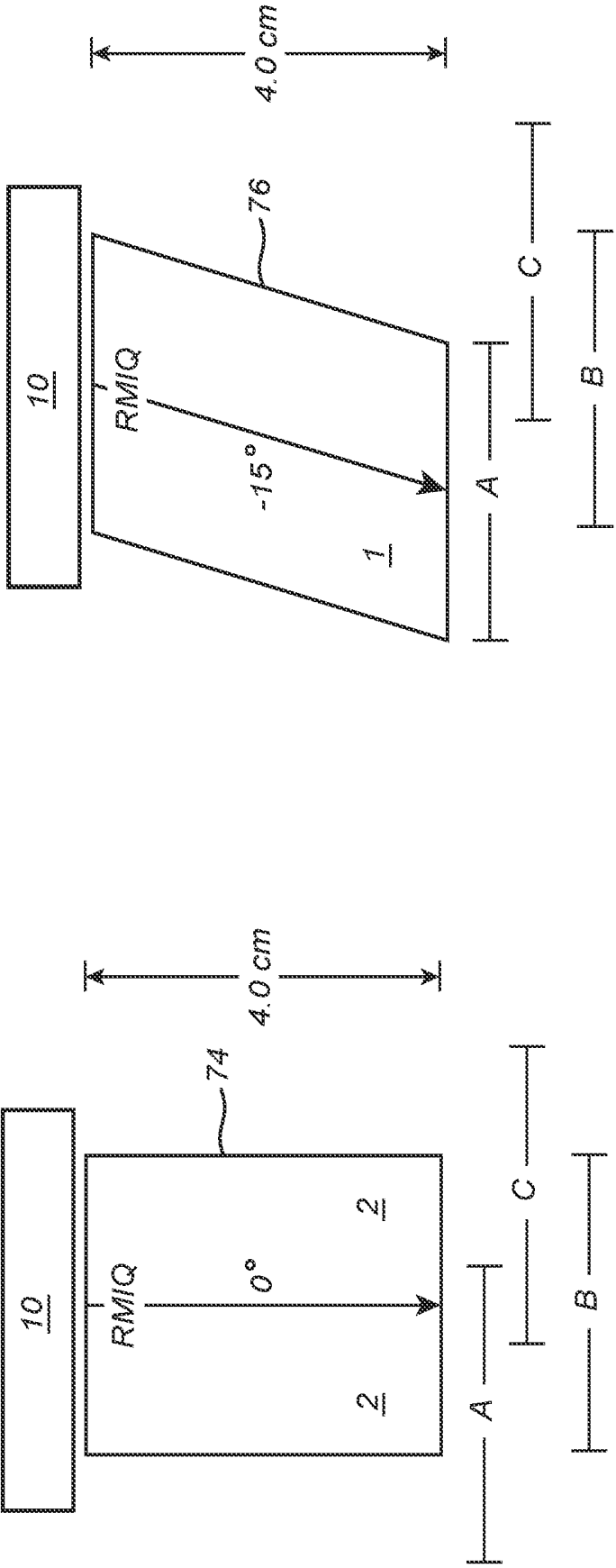


Fig. 3c

Fig. 3d

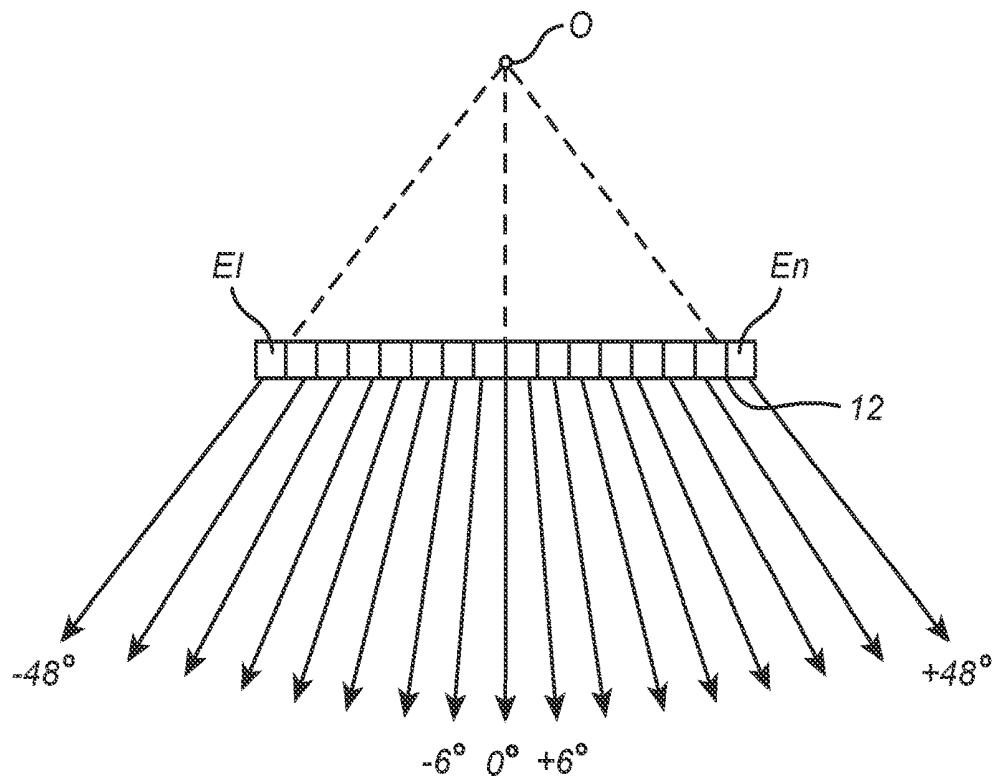


Fig. 4a

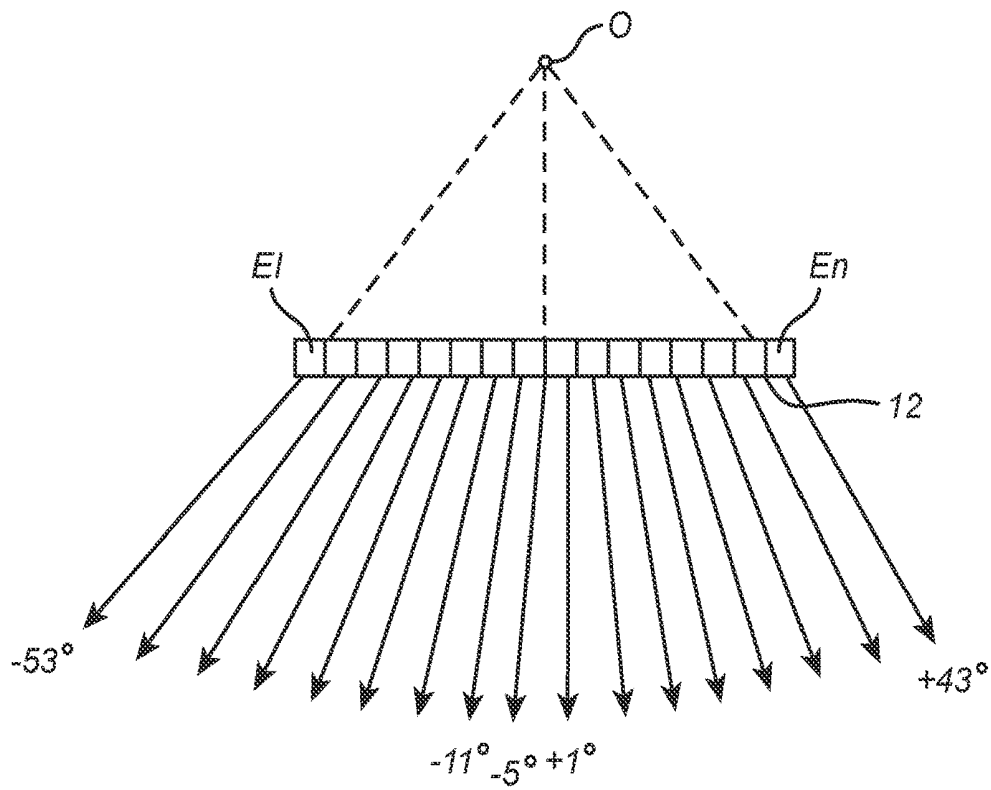


Fig. 4b

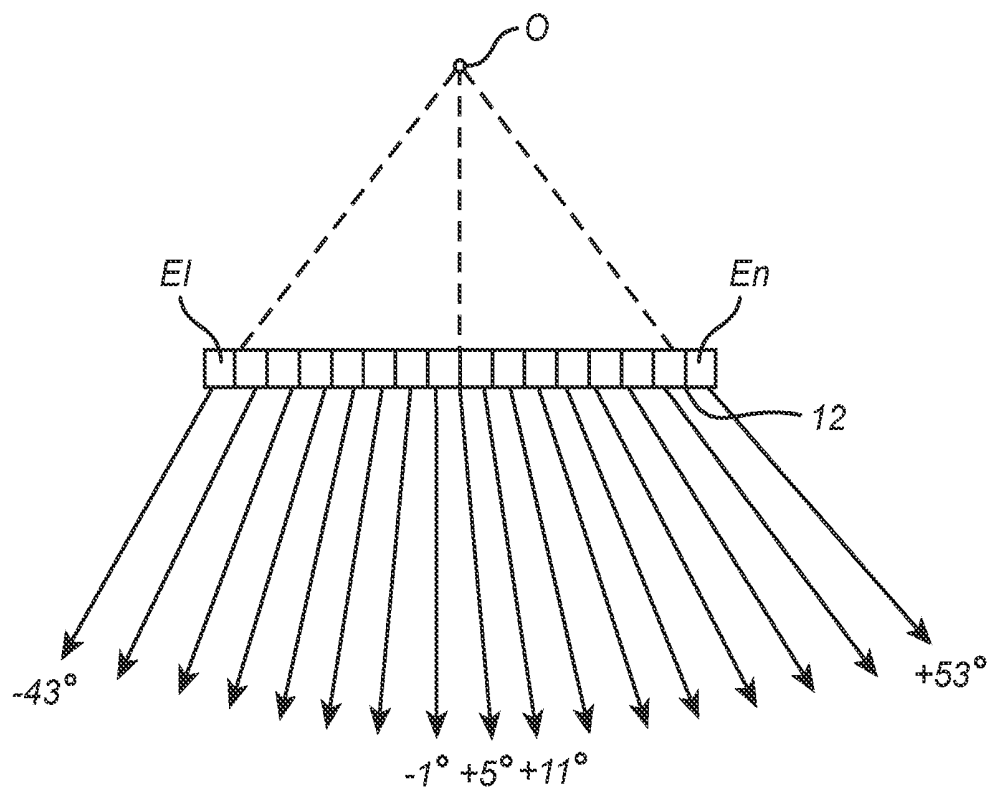


Fig. 4c

ULTRASONIC DIAGNOSTIC IMAGING SYSTEM WITH SPATIAL COMPOUNDING OF TRAPEZOIDAL SECTOR

This application is the U.S. National Phase application under 35 U.S.C. § 371 of International Application No. PCT/IB2014/060079, filed on Mar. 24, 2014, which claims the benefit of U.S. Application No. 61/804,783 filed on Mar. 25, 2013. These applications are hereby incorporated by reference herein.

This invention relates to ultrasonic diagnostic imaging systems and, in particular, to ultrasonic diagnostic imaging systems which produce spatially compounded images in a trapezoidal sector format.

Spatial compounding is an imaging technique in which a number of ultrasound images of a given target that have been obtained from multiple vantage points or angles (look directions) are combined into a single compounded image by combining the data received from each point in the compound image target which has been received from each angle or look direction. Examples of spatial compounding may be found in U.S. Pat. No. 4,649,327 (Fehr et al.); U.S. Pat. No. 4,319,489 (Yamaguchi et al.); U.S. Pat. No. 4,159,462 (Rocha et al.); U.S. Pat. No. 6,210,328 (Robinson et al.) U.S. Pat. No. 6,126,598 (Entrekin et al.) and U.S. Pat. No. 6,224,552 (Jago et al.) Real time spatial compound imaging is performed by rapidly acquiring a series of partially overlapping component image frames from substantially independent spatial directions, utilizing an array transducer to implement electronic beam steering and/or electronic translation of the component frames. The component frames are combined into a compound image by summation, averaging, peak detection, or other combinational means. The acquisition sequence and formation of compound images are repeated continuously at a rate limited by the acquisition frame rate, that is, the time required to acquire the full complement of scanlines of the component frames over the selected width and depth of imaging. The compounded image typically shows lower speckle and better specular reflector delineation than conventional ultrasound images from a single viewpoint. Speckle is reduced (i.e., speckle signal to noise ratio is improved) by the square root of N in a compound image with N component frames, provided that the component frames used to create the compound image are substantially independent and are averaged. Several criteria can be used to determine the degree of independence of the component frames (see, e.g., O'Donnell et al. in IEEE Trans. UFFC v. 35, no. 4, pp 470-76 (1988)). In practice, for spatial compound imaging with a steered linear array, this implies a minimum steering angle between component frames. This minimum angle is typically on the order of several degrees, e.g., three or four degrees.

The second way that spatial compound scanning improves image quality is by improving the acquisition of specular interfaces. For example, a curved bone-soft tissue interface produces a strong echo when the ultrasound beam is exactly perpendicular to the interface, and a very weak echo when the beam is only a few degrees off perpendicular. These interfaces are often curved, and with conventional scanning only a small portion of the interface is visible. Spatial compound scanning acquires views of the interface from many different angles, making the curved interface visible and continuous over a larger field of view. Greater angular diversity generally improves the continuity of specular targets. However, the angular diversity available is limited by the acceptance angle of the transducer array elements. The

acceptance angle depends on the transducer array element pitch, frequency, and construction methods.

Spatial compounding can be done in the various image formats used in ultrasonic imaging including sector images and linear images. A convenient format for spatial compounding is the steered linear format as described in the aforementioned Robinson et al., Entrekin et al., and Jago et al. patents. In this format each component frame is formed from parallel scanlines steered in a given look direction. For example, a first component frame can be acquired using scanlines all steered in the 0° (straight ahead) direction. Second and third component frames can then be acquired with all scanlines steered in the +15° direction and the -15° direction, respectively. When the component frames are combined in spatial alignment they will produce a trapezoidal-shaped image which is spatially compounded. Unfortunately, as discussed below, the spatial compounding effect is not uniform throughout the image. This is because there are different degrees of image overlap in different areas of the combined image. Accordingly it is desirable to do spatial compounding in a trapezoidal scan format in which the spatial compounding effect combines the greatest number of component frames throughout the largest extent of the spatially compounded image.

In accordance with the principles of the present invention, spatially compounded trapezoidal images are formed by scanning virtual apex component frames. Virtual apex is a phased beam steering technique in which the scanlines that scan the image field are steered at different angles. It is called virtual apex because all of the scanlines appear to emanate from a common point or apex behind the face of the ultrasound transducer. Component frames are acquired in the virtual apex format with the scanlines steered at differing angles relative to the face of the transducer in each component frame. When the component frames are combined the overlap over a substantial portion of the image field, providing a high degree of spatial compounding throughout a large region of the compounded image.

In the drawings:

FIG. 1 illustrates in block diagram form an ultrasonic diagnostic imaging system constructed in accordance with the principles of the present invention;

FIG. 2 illustrates in block diagram form an implementation of the spatial compounding processor of FIG. 1;

FIGS. 3a through 3d illustrate the region of maximum image quality of a spatially compounded image formed by component frames acquired in the steered linear scan format; and

FIGS. 4a through 4c illustrates component frames acquired for formation of a spatially compounded trapezoidal image in accordance with the present invention.

Referring first to FIG. 1, an ultrasonic diagnostic imaging system constructed in accordance with the principles of the present invention is shown. An ultrasound probe 10 including a planar array transducer 12 which transmits beams at different angles over an image field denoted by the dashed rectangle and parallelograms outlining regions scanned by steered linear beam scanning. Three groups of scanlines are indicated in the drawing, labeled A, B, and C with each group being steered at a different angle relative to the face of the array transducer. The array transducer can be a one dimensional (1D) array of transducer elements or a two dimensional (2D) matrix array of transducer elements. The transmission of the beams is controlled by a transmitter 14 which controls the phasing and time of actuation of each of the elements of the array transducer so as to transmit each beam from a predetermined origin along the array and at a

predetermined angle. When a 2D array transducer is used, transmission and partial beamforming is provided by a microbeamformer IC (μ BF) located in the probe **10**. A 1D array transducer can also use a microbeamformer if desired. The echoes returned from along each scanline are received by the elements of the array, digitized as by analog to digital conversion, and coupled to a digital beamformer **16**. When a microbeamformer is used, at least partial beamforming is performed in the probe by the microbeamformer before the signals are coupled to the system beamformer **16**. The digital beamformer delays and sums the echoes from the array elements or microbeamformer to form a sequence of focused, coherent digital echo samples along each scanline. The transmitter **14**, microbeamformer and beamformer **16** are operated under control of a system controller **18**, which in turn is responsive to the settings of controls on a user interface **20** operated by the user of the ultrasound system. The system controller controls the transmitter (and/or microbeamformer) to transmit the desired number of scanline groups at the desired angles, transmit energies and frequencies. The system controller also controls the digital beamformer to properly delay and combine the received echo signals for the apertures and image depths used.

The scanline echo signals are filtered by a programmable digital filter **22**, which defines the band of frequencies of interest. When imaging harmonic contrast agents or performing tissue harmonic imaging the passband of the filter **22** is set to pass harmonics of the transmit band. The filtered signals are then detected by a detector **24**. In a preferred embodiment the filter and detector include multiple filters and detectors so that the received signals may be separated into multiple passbands, individually detected and recombined to reduce image speckle by frequency compounding. For B mode imaging the detector **24** will perform amplitude detection of the echo signal envelope. For Doppler imaging ensembles of echoes are assembled for each point in the image and are Doppler processed to estimate the Doppler shift or Doppler power intensity.

In accordance with the principles of the present invention the digital echo signals are processed by spatial compounding in a processor **30**. The digital echo signals are initially pre-processed by a preprocessor **32**. The pre-processor **32** can preweight the signal samples if desired with a weighting factor. The samples can be preweighted with a weighting factor that is a function of the number of component frames used to form a particular compound image. The pre-processor can also weight edge lines that are at the edge of one overlapping image so as to smooth the transitions where the number of samples or images which are compounded changes. The pre-processed signal samples may then undergo a resampling in a resampler **34**. The resampler **34** can spatially realign the estimates of one component frame or to the pixels of the display space.

After resampling the image frames are compounded by a combiner **36**. Combining may comprise summation, averaging, peak detection, or other combinational means. The samples being combined may also be weighted prior to combining in this step of the process. Finally, post-processing is performed by a post-processor **38**. The post-processor normalizes the combined values to a display range of values. Post-processing can be most easily implemented by look-up tables and can simultaneously perform compression and mapping of the range of compounded values to a range of values suitable for display of the compounded image.

The compounding process may be performed in estimate data space or in display pixel space. In a preferred embodiment scan conversion is done following the compounding

process by a scan converter **40**. The compound images may be stored in a Cineloop® memory **42** in either estimate or display pixel form. If stored in estimate form the images may be scan converted when replayed from the Cineloop memory for display. The scan converter and Cineloop memory may also be used to render three dimensional presentations of the spatially compounded images as described in U.S. Pat. Nos. 5,485,842 and 5,860,924. Following scan conversion the spatially compounded images are processed for display by a video processor **44** and displayed on an image display **50**.

FIG. 2 illustrates one implementation of the spatial compounding processor **30** of FIG. 1. The processor **30** in this example is implemented by one or more digital signal processors **60** which process the image data in various ways. The digital signal processors **60** weights the received image data and can resample the image data to spatially align pixels from frame to frame, for instance. The digital signal processors **60** direct the processed image frames to a plurality of frame memories **62** which buffer the individual component image frames. The number of component image frames capable of being stored by the frame memories **62** is preferably at least equal to the maximum number of component image frames to be compounded such as sixteen frames. In accordance with the principles of the present invention, the digital signal processors are responsive to control parameters including image display depth, depth of region of greatest compounding, clinical application, compound display rate, mode of operation, and acquisition rate for determining the number of images to compound at a given instant in time. The digital signal processors select component frames stored in the frame memories **62** for assembly as a compound image in accumulator memory **64**. The compounded image formed in the accumulator memory **64** is weighted or mapped by a normalization circuit **66**, then compressed to the desired number of display bits and, if desired, remapped by a lookup table (LUT) **68**. The fully processed compounded image data is then transmitted to the scan converter for formatting and display.

Compound scanning with a steered linear array results in a pattern of overlapping component frames such that the region of maximum image quality (RMIQ) where all N frames overlap is an inverted triangular region with its base at the top of the compound image. With other scanning geometries such as overlapping phased array frames emanating from different points of the array, the RMIQ will exhibit a correspondingly different shape. This is illustrated by FIGS. 3a through 3d. FIGS. 3b, 3c, and 3d illustrate component steered linear frames which are combined to form the spatially compounded image of FIG. 3a. The component frame of FIG. 3b is formed by a plurality of parallel, adjacent scanlines which scan the parallelogram-shaped image field **72** at an angle of +15°, one of which is shown in the center of the image frame **72**. This is component frame "C" of the compounded image. The component frame of FIG. 3c is formed by a plurality of parallel, adjacent scanlines which scan the rectangular-shaped image field **74** at an angle of 0°, one of which is shown in the center of the image frame **74**. This is component frame "B" of the compounded image. The component frame of FIG. 3d is formed by a plurality of parallel, adjacent scanlines which scan the parallelogram-shaped image field **76** at an angle of -15°, one of which is shown in the center of the image frame **76**. This is component frame "A" of the compounded image. In FIG. 3a the three component frames A, B, and C are shown when spatially registered to form the final compounded image **80**. On either side of the RMIQ region,

where all three component frames overlap and are compounded, the number of overlapping frames decreases spatially, with only two frames overlapping in the regions designated 2 and single frames present in the regions designated 1. This means that a particular point in the compounded image may only receive contributions from a sub-set of the component frames, depending on whether a component frame has data at that point.

In accordance with the principles of the present invention a spatially compounded ultrasound image is produced from component frames scanned in a virtual apex scan format. Virtual apex is a form of phased array scanning in which the beams are steered at progressively different angles relative to the face (emitting surface) of the transducer array. In conventional phased array imaging all of the beams emanate from a common point on the face of the array, generally at the center of the array. This common point is the apex of a triangular-shaped sector image. In virtual apex scanning the common point from which the scanlines emanate is a "virtual" point located behind the face of the array as described in U.S. Pat. No. 5,123,415 (Daigle). Such a scan format is shown in FIG. 4a, where the virtual apex is the point "0" behind the face of the array 12. The transducer array in this example is a linear 1D array, a single line of transducer elements E1 to En. As is seen in this example the center scanline is transmitted and received at an angle of 0° relative to the face of the array. The angle convention used in ultrasound scanning designates the straight-ahead direction in front of the array as the 0° direction. On either side of this center scanline the adjacent scanlines are progressively steered at ever-increasing angles. In this example the scanline immediately to the left of center is steered at an angle of -6° and the scanline immediately to the right of center is steered at an angle of +6°. The inclination of steering angles increases in increments of 6° with increasing distance from the center of the array to a maximum scanline angle of -48° and +48° at the lateral sides of the scanned sector-shaped image field.

The scan format of FIG. 4a produces one component frame for spatial compounding in this example. Two other component frames are shown in FIGS. 4b and 4c. In FIG. 4b each scanline emanates from the same point on the face of the array as the scanlines in FIG. 4a, but are steered in different look directions of 5° to the left. The scanline which was steered at an angle of 0° in FIG. 4a is steered at an angle of -5° in FIG. 4b. This scanline now interrogates the image field in a different look direction than the 0° scanline of FIG. 4a. The 5° difference in look direction provides a diversity in look direction sufficient to produce the speckle reduction characteristic of a spatially compounded image. Similarly, the scanline to the left of center which was formerly steered at an angle of -6° is now steered an addition increment of 5° so that it is directed at an angle of -11°. The scanline to the right of center, formerly steered at an angle of +6°, is now steered at an angle of +1°. This incremental change in steering angles is carried out across the image field and the scanline to the left lateral side of the sector is steered at an angle of -53° and the scanline on the right lateral side is steered at an angle of +43°. Thus, each point in the image field in FIG. 4b is interrogated from a different look direction than that effected by the scan format of FIG. 4a.

In FIG. 4c each scanline again emanates from the same point on the face of the array as in the previous component frames, but this time at an angular increment of 5° to the right. Thus, the 0° scanline of FIG. 4a is now steered at an angle of +5°. The scanline to the left of center that was steered at an angle of -6° in FIG. 4a is now steered at an

angle of -1° in FIG. 4c, and the scanline to the right that was steered at an angle of +6° is now steered at an angle of +11°. This 5° incremental inclination of each scanline is repeated across the image field, resulting in the left-most scanline being steered at a -43° angle and the right-most scanline being steered at an angle of +53°. This results in each point in the image field being interrogated at a third look direction which is different from that of both the first and second component images.

When the three component images of FIGS. 4a, 4b, and 4c are compounded, there is a compounding of three component images across virtually the entire area of the image. Stated another way, the RMIQ exists over virtually the entire image field. It is only at the lateral extremes of the image where the RMIQ falls off. The inventive spatial compounding technique is effective for both two and three dimensional imaging, it can be performed with both standard phased array scanning and virtual apex phased scanning, and it can be performed with scan converted or pre-scan converted image data. While it is generally more convenient to acquire each component frame in its entirety before scanning another component frame, those skilled in the art will recognize that the scanlines of different component frames can be acquired in a time-interleaved manner. For example, a scanline emanating from one point on the face of the array can be acquired in a first look direction for one component frame, a scanline emanating from the same point can be acquired in a second look direction for a second component frame, and a scanline emanating from the same point can be acquired in a third look direction for a third component frame. The component frames are then assembled from these time-interleaved scanlines.

What is claimed is:

1. An ultrasonic diagnostic imaging system for producing spatially compounded images, including:

an array transducer adapted to acquire component frames at a plurality of different look directions, and
a compound image processor comprising:

a transmitter adapted to control the array transducer to steer scanlines in a trapezoidal scan format for each of a plurality of component frames, wherein the scan format for each of the plurality of component frames is defined by scanlines including a center scanline, and a first plurality of adjacent scanlines and a second plurality of adjacent scanlines at uniform angular increments to the left and right, respectively, of the center scanline, wherein the transmitter is adapted to generate the plurality of different look directions by steering scanlines of each component frame over a plurality of different scan angles such that the scanlines of each component frame are steered at uniformly incremented scan angles to the left or right of respective scanlines of adjacent component frames such that each point in an image field is interrogated by at least three of the plurality of different look directions; and

a compound image memory for storing adapted to store component frames which have been acquired from different look directions,

wherein the compound image processor is adapted to combine the acquired component frames to form a spatially compounded image.

2. The ultrasonic diagnostic imaging system of claim 1, further comprising a beamformer adapted to receive echo signals from each scanline direction.

3. The ultrasonic diagnostic imaging system of claim 2, wherein the transmitter further comprises a microbeam-

7

former, wherein the array transducer and the microbeam-former are both located in an ultrasound probe.

4. The ultrasonic diagnostic imaging system of claim 2, wherein the beamformer further comprises a microbeam-former, wherein the array transducer and the microbeam-former are both located in an ultrasound probe.

5. The ultrasonic diagnostic imaging system of claim 1, wherein the array transducer further comprises a one dimensional linear array of transducer elements.

6. The ultrasonic diagnostic imaging system of claim 1, wherein the array transducer further comprises a two dimensional planar array of transducer elements.

7. The ultrasonic diagnostic imaging system of claim 1, wherein the respective scanlines of each component frame emanate from the same points on the face of the array transducer.

8. The ultrasonic diagnostic imaging system of claim 1, wherein the transmitter is further adapted to steer respective scanlines of each component frame, which emanate from the same point on the face of the array transducer, at different steering angles.

9. The ultrasonic diagnostic imaging system of claim 1, wherein the trapezoidal scan format further comprises a near field region in front of the face of the array transducer in which the scanlines converge to a common apex.

8

10. The ultrasonic diagnostic imaging system of claim 1, wherein the transmitter is further adapted to control the array transducer to steer the scanlines of each component frame by phased array beam steering.

11. The ultrasonic diagnostic imaging system of claim 1, wherein the transmitter is further adapted to control the array transducer to steer the scanlines of each component frame in a virtual apex scan format.

12. The ultrasonic diagnostic imaging system of claim 1, wherein the array transducer is adapted to acquire scanlines of the component frames in a time-interleaved sequence.

13. The ultrasonic diagnostic imaging system of claim 1, wherein the array transducer is adapted to acquire a look direction diversity between the component frames of at least three degrees.

14. The ultrasonic diagnostic imaging system of claim 13, wherein the look direction diversity between the component frames is five degrees.

15. The ultrasonic diagnostic imaging system of claim 1, wherein the compound image processor is adapted to combine the acquired component frames by one of summation, averaging, peak detection, or other combinational means.

* * * * *

专利名称(译)	梯形扇形空间复合的超声诊断成像系统		
公开(公告)号	US10345444	公开(公告)日	2019-07-09
申请号	US14/778292	申请日	2014-03-24
[标]申请(专利权)人(译)	皇家飞利浦电子股份有限公司		
申请(专利权)人(译)	皇家飞利浦N.V.		
当前申请(专利权)人(译)	皇家飞利浦N.V.		
[标]发明人	OLSSON LARS JONAS		
发明人	OLSSON, LARS JONAS		
IPC分类号	G01S15/89 G01S7/52 A61B8/08 A61B8/14 A61B8/00		
CPC分类号	G01S15/8995 A61B8/14 A61B8/4444 A61B8/4494 A61B8/461 G01S15/8925 A61B8/5207 A61B8/5238 G01S7/52085 G01S15/8918 A61B8/488 A61B8/52 G01N29/04		
优先权	61/804783 2013-03-25 US		
其他公开文献	US20160282467A1		
外部链接	Espacenet		

摘要(译)

超声诊断成像系统通过组合从不同观察方向获取的分量帧来产生空间复合的梯形扇区图像。使用虚拟顶点扫描格式，使得组件框架的每个扫描线从阵列换能器（12）面上的不同点（E1，En）发出，并以不同的扫描角度转向。对于不同的分量帧，扫描线分别以不同的角度转向。在所示示例中，每个分量帧的扫描线相对于参考分量帧中的对应扫描线递增五度。当组合帧组合用于空间复合时，组件帧的最大数量实际上在整个图像场上组合。

