



US010372399B2

(12) **United States Patent**  
**Rust et al.**

(10) **Patent No.:** **US 10,372,399 B2**  
(45) **Date of Patent:** **\*Aug. 6, 2019**

(54) **ULTRASOUND IMAGE DISPLAY SET-UP FOR REMOTE DISPLAY TERMINAL**

(52) **U.S. Cl.**  
CPC ..... **G06F 3/1423** (2013.01); **A61B 8/463** (2013.01); **A61B 8/565** (2013.01); **G01S 7/003** (2013.01);

(71) Applicant: **KONINKLIJKE PHILIPS N.V.**,  
Eindhoven (NL)

(Continued)

(72) Inventors: **David Rust**, Seattle, WA (US); **Karl Erhard Thiele**, Andover, MA (US); **Kevin Bradley**, Bothell, WA (US); **Earl M. Canfield**, Snohomish, WA (US)

(58) **Field of Classification Search**  
CPC ..... G06F 19/34; G06F 19/32  
See application file for complete search history.

(73) Assignee: **Koninklijke Philips N.V.**, Eindhoven (NL)

(56) **References Cited**

U.S. PATENT DOCUMENTS

5,474,073 A 12/1995 Schwartz  
5,485,842 A 1/1996 Quistgaard

(Continued)

(\* ) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 0 days.

This patent is subject to a terminal disclaimer.

FOREIGN PATENT DOCUMENTS

RU 2152173 C1 10/2000  
WO 2006008664 A1 1/2006

(Continued)

*Primary Examiner* — Alexander Eisen  
*Assistant Examiner* — Cory A Almeida

(21) Appl. No.: **15/871,164**

(22) Filed: **Jan. 15, 2018**

(65) **Prior Publication Data**

US 2018/0136896 A1 May 17, 2018

**Related U.S. Application Data**

(63) Continuation of application No. 15/585,271, filed on May 3, 2017, now Pat. No. 9,898,242, which is a (Continued)

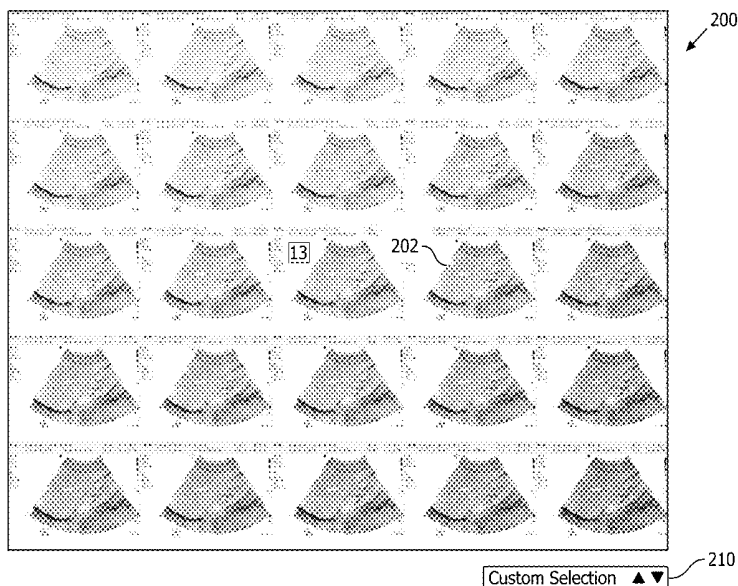
(51) **Int. Cl.**  
**G06F 19/00** (2018.01)  
**G06F 3/14** (2006.01)

(Continued)

(57) **ABSTRACT**

An ultrasound system enables simplified setup of a remote terminal for display of ultrasound images acquired by the ultrasound system. An image acquired by the ultrasound system is processed by or with display parameters for different viewing conditions or devices, such as display gamma correction, ambient lighting, or image quality. A plurality of versions of an image with slightly different display appearances are exported to the remote terminal, where a viewer can view all of the image versions simultaneously. The viewer selects the best image, and the display characteristics of the selected image are used for images subsequently exported from the ultrasound system to the remote terminal.

**15 Claims, 5 Drawing Sheets**



- Related U.S. Application Data**
- continuation of application No. 14/402,353, filed as application No. PCT/IB2013/053788 on May 10, 2013, now Pat. No. 9,678,702.
- (60) Provisional application No. 61/650,241, filed on May 22, 2012.
- (51) **Int. Cl.**  
*G16H 40/40* (2018.01)  
*G01S 7/00* (2006.01)  
*G01S 7/52* (2006.01)  
*A61B 8/00* (2006.01)  
*G09G 5/14* (2006.01)  
*G16H 30/20* (2018.01)  
*G16H 30/40* (2018.01)
- (52) **U.S. Cl.**  
 CPC ..... *G01S 7/52053* (2013.01); *G01S 7/52084* (2013.01); *G06F 3/1454* (2013.01); *G06F 19/321* (2013.01); *G09G 5/14* (2013.01); *G16H 30/20* (2018.01); *G16H 30/40* (2018.01); *G16H 40/40* (2018.01); *A61B 8/464* (2013.01); *F04C 2270/041* (2013.01); *G09G 2354/00* (2013.01); *G09G 2380/08* (2013.01)

- References Cited**
- U.S. PATENT DOCUMENTS
- |              |      |         |                  |                               |
|--------------|------|---------|------------------|-------------------------------|
| 5,720,291    | A    | 2/1998  | Schwartz         |                               |
| 5,833,613    | A    | 11/1998 | Averkiou         |                               |
| 6,013,032    | A    | 1/2000  | Savord           |                               |
| 6,186,950    | B1   | 2/2001  | Averkiou         |                               |
| 6,375,617    | B1   | 4/2002  | Fraser           |                               |
| 6,692,438    | B2   | 2/2004  | Skyba            |                               |
| 6,951,543    | B2   | 10/2005 | Roundhill        |                               |
| 2004/0061889 | A1 * | 4/2004  | Wood             | ..... G06F 19/321<br>358/1.15 |
| 2005/0275666 | A1 * | 12/2005 | Nagarajan        | ..... H04N 1/00209<br>345/660 |
| 2008/0097203 | A1 * | 4/2008  | Nereson          | ..... G01S 7/52053<br>600/437 |
| 2010/0189329 | A1   | 7/2010  | Mo et al.        |                               |
| 2011/0196237 | A1   | 8/2011  | Pelissier et al. |                               |
| 2011/0279477 | A1   | 11/2011 | Wang et al.      |                               |
| 2012/0108960 | A1 * | 5/2012  | Halmann          | ..... A61B 8/461<br>600/437   |
| 2013/0012820 | A1 * | 1/2013  | Brown            | ..... A61B 8/465<br>600/443   |
- FOREIGN PATENT DOCUMENTS
- |    |               |    |        |
|----|---------------|----|--------|
| WO | 2008007301    | A2 | 1/2008 |
| WO | 2011117788    | A1 | 9/2011 |
| WO | WO-2011117788 | *  | 9/2011 |
- \* cited by examiner

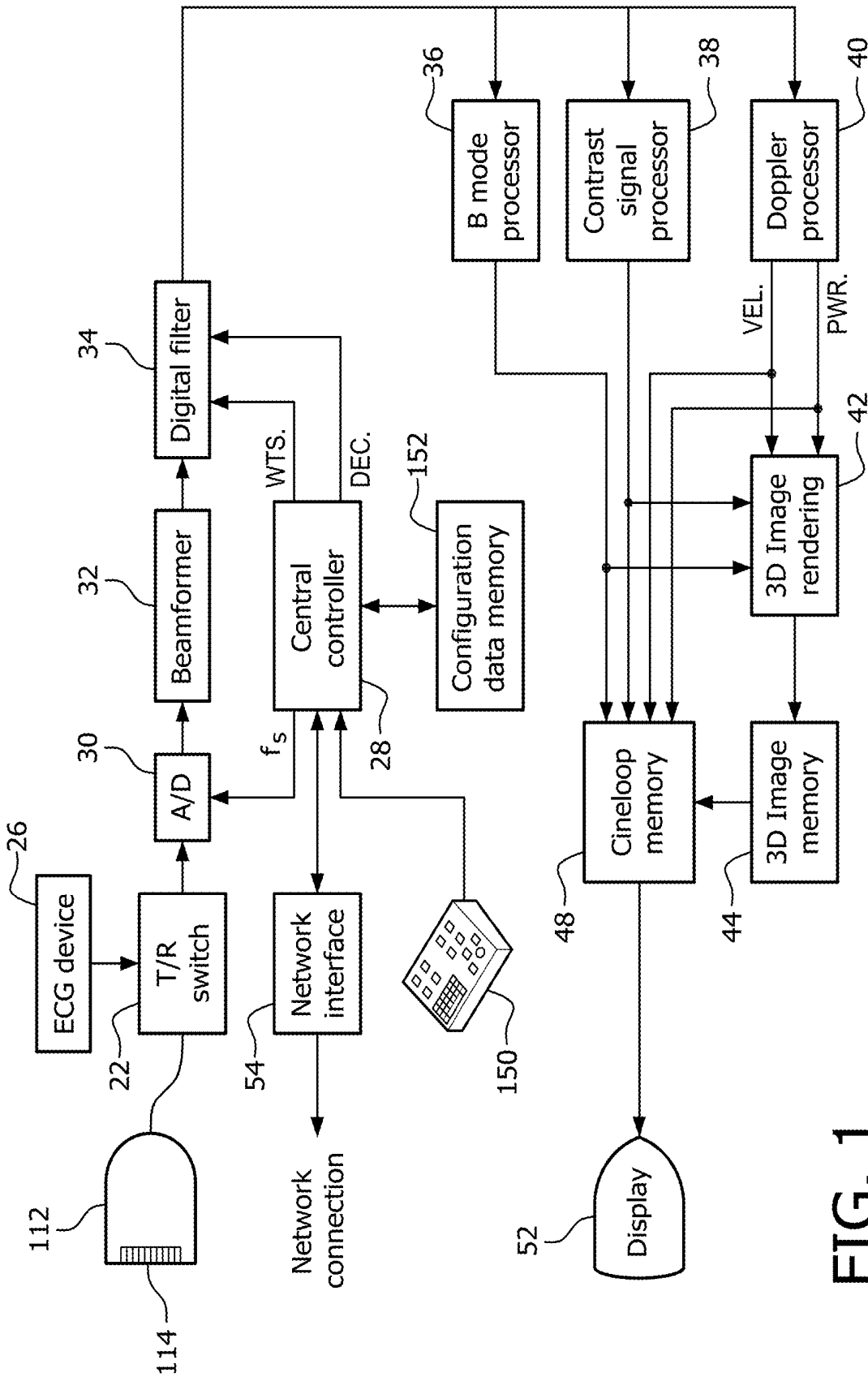


FIG. 1

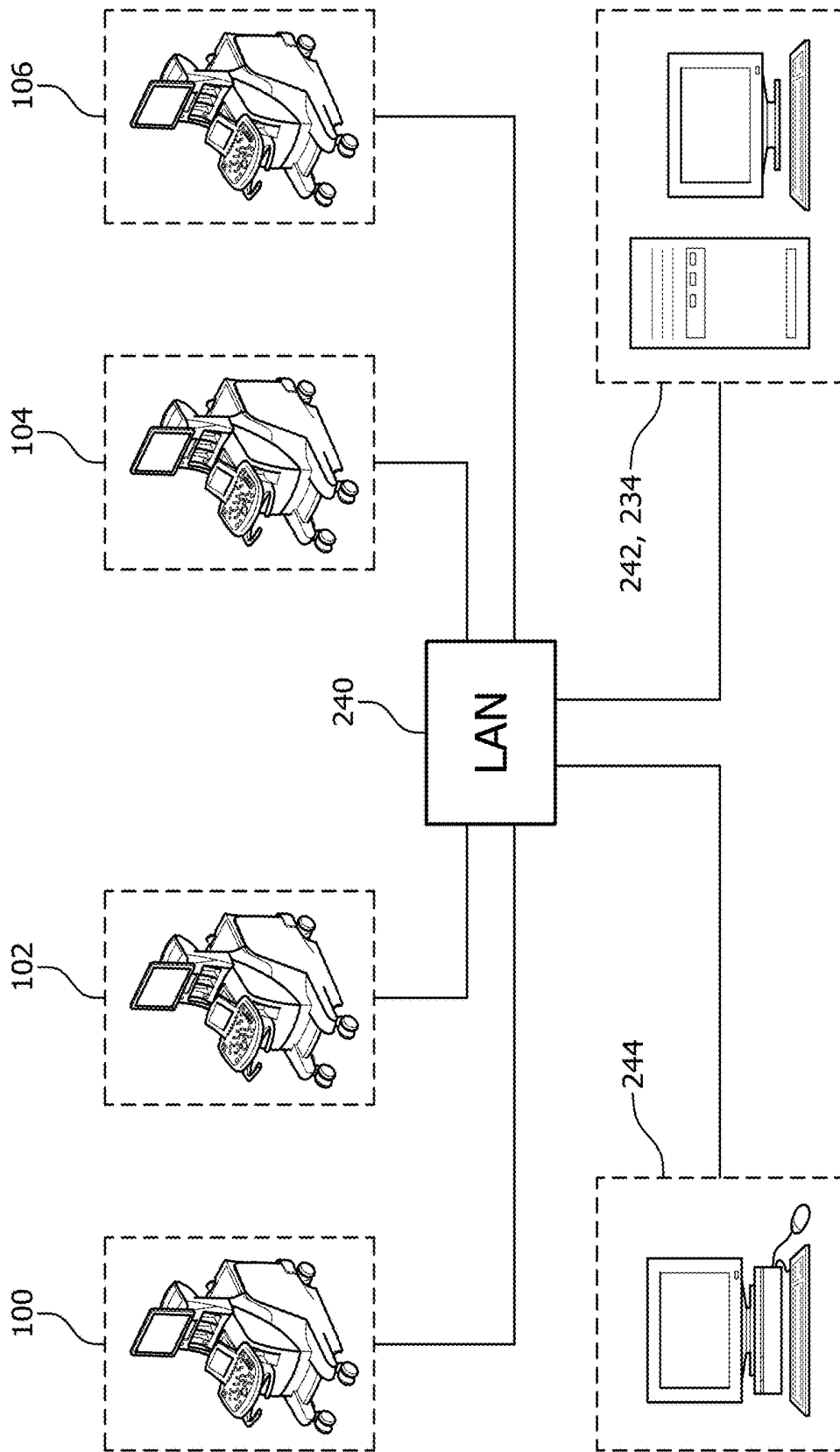


FIG. 2

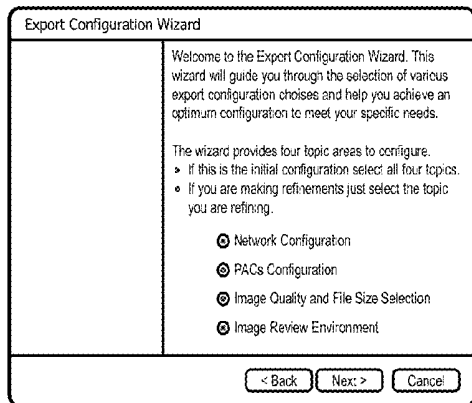


FIG. 3a

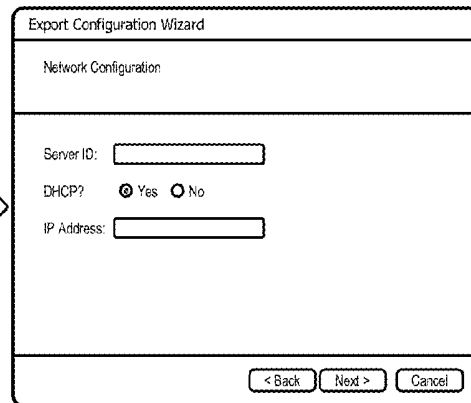


FIG. 3b

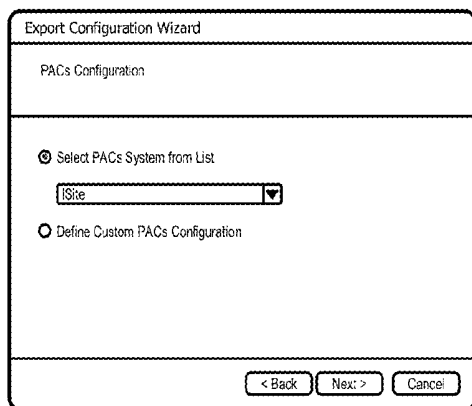


FIG. 3c

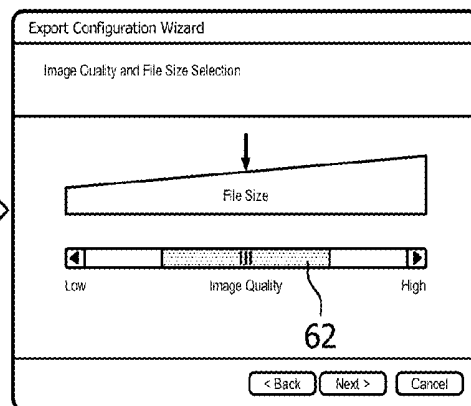


FIG. 3d

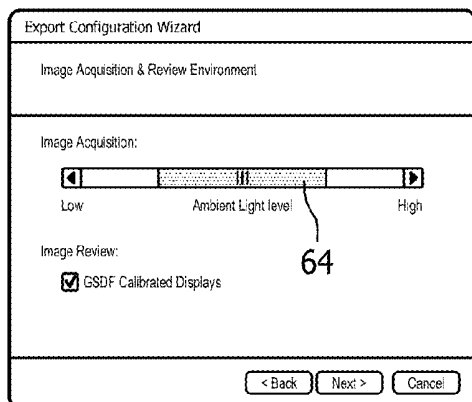


FIG. 3e

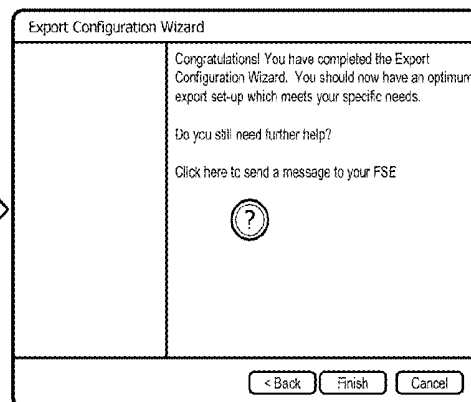


FIG. 3f

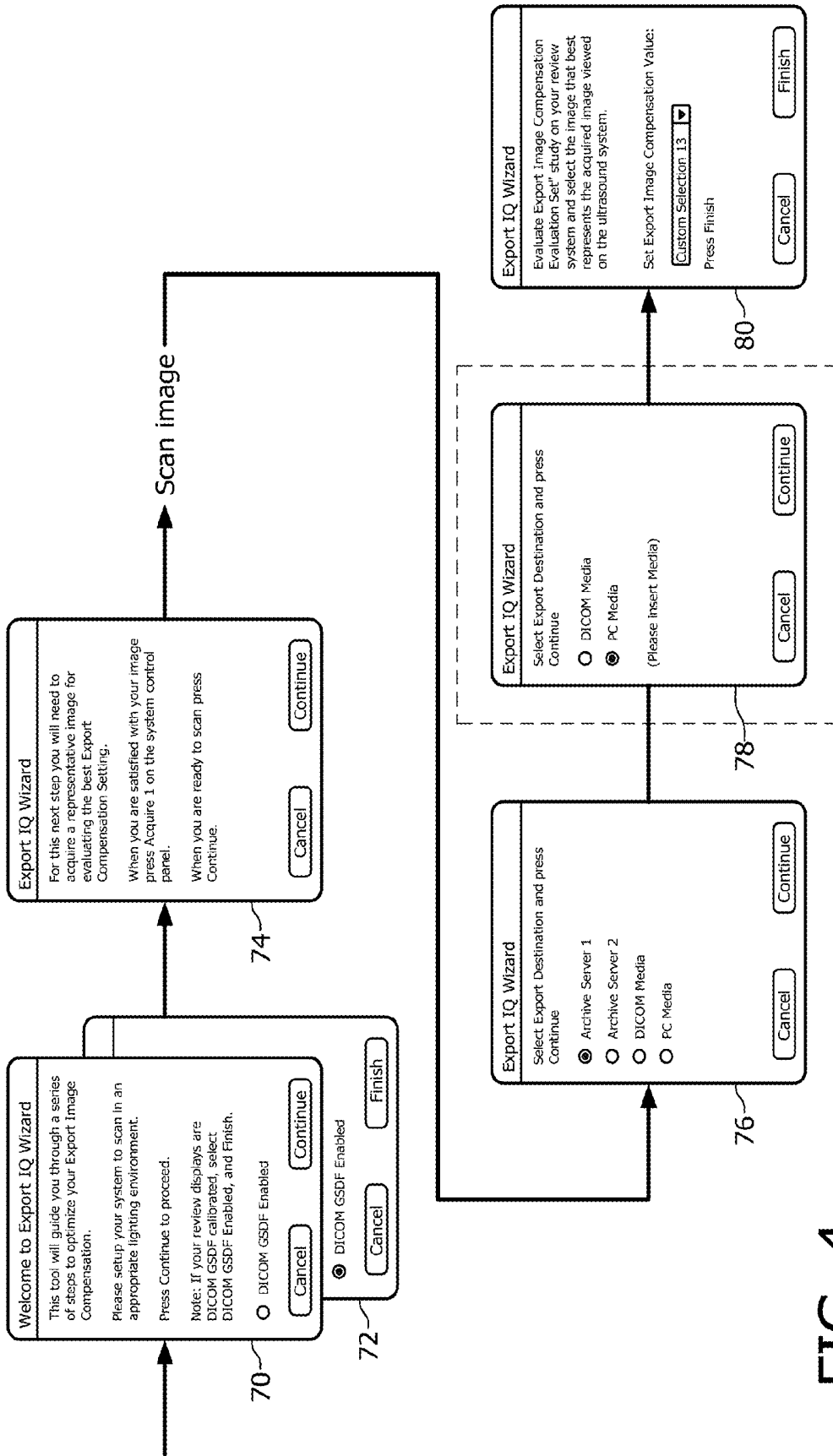


FIG. 4

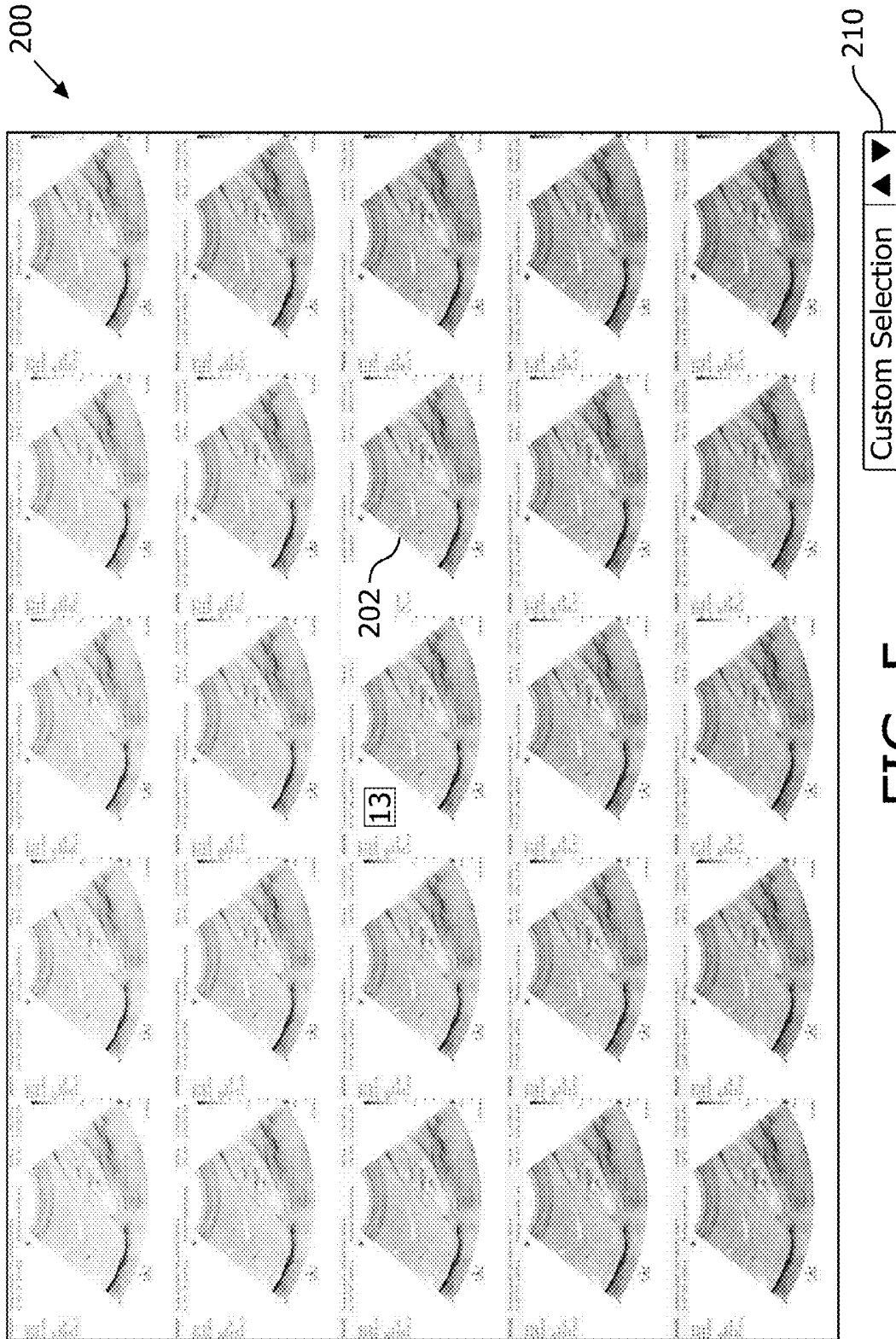


FIG. 5

## ULTRASOUND IMAGE DISPLAY SET-UP FOR REMOTE DISPLAY TERMINAL

This application is a continuation application of U.S. patent application Ser. No. 15/585,271 filed May 3, 2017 which is a continuation application of Ser. No. 14/402,353 filed Nov. 20, 2014, which is a national stage filing under 35 U.S.C. § 371(c) of International Appl. No. PCT/IB2013/053788, filed Mar. 11, 2013, which claims priority to U.S. Prov. Appl. No. 61/650,241, filed May 22, 2012, the disclosures of which are incorporated herein by reference in their entirety.

This invention relates to medical diagnostic ultrasound systems and, in particular, to the export and display of images from an ultrasound system to a remote display terminal such as a review station on a PACS (picture archiving and communication) system.

A typical ultrasonic imaging system will have dozens of control setting which can be adjusted by a user to best display an image of anatomy of the body. For instance, when imaging tissue a sonographer will be able to set the line density, focal zones, dynamic range, transmit and receive frequencies, resolution penetration, transmit power, sector width, grayscale mapping, number of multilines, and numerous other imaging variables. When imaging blood flow in the colorflow mode some of the imaging variables which may be adjusted are wall filter settings, color map, frame rate, velocity range, frequency compounding, filter settings, and Doppler steering angle. With so many possible settings it is not surprising that ultrasound systems have control software that stores parameter presets for different types of imaging exams. A sonographer starting an obstetrical exam, for example, can select the presets for an OB exam and the ultrasound system will invoke a set of presets commonly used for most OB exams. The sonographer may be satisfied and use the system-selected presets, or can adjust the preset values and save the new set of presets as his or her preferred presets for a particular patient or type of exam.

Unless a sonographer is always satisfied by the system presets for an exam type, even customizing and saving sets of preset parameters for different exams can be a time consuming task. Moreover even custom presets can become unsatisfactory or obsolete as equipment is upgraded and new probes become available for standard exams. However, U.S. Pat. No. 6,951,543 (Roundhill) has provided a solution to this problem. That is to process an ultrasound image with a variety of different parameter values, such as the standard system preset values and common variations thereof. The sonographer does not have adjust numerous parameters and controls and see what difference each incremental or new parameter variation produces. Instead, the sonographer views a gallery of images, each of which has been processed by at least a slightly different set of acquisition or image processing parameters. The sonographer then simply picks the image that looks the best, and the parameters of that image are then applied for a particular exam. The selection process is far simpler than painstakingly adjusting numerous ultrasound system parameters.

The reading of ultrasound images in order to arrive at a diagnosis of a disease condition often does not occur on the ultrasound system which acquired the images. In many hospitals and clinics a sonographer may acquire the ultrasound images by scanning a patient, and the images of the patient are then transmitted to a diagnostic workstation or terminal where a cardiologist or radiologist will view the images, make a diagnosis, and prepare a diagnostic report. At times the images may be stored on a PACS archive server

from which a physician can access the images for diagnosis. The workstation or terminal where the images are read may be equipped with special diagnostic software such as the QLAB diagnostic ultrasound analysis software package available from Philips Healthcare in Andover, Mass., USA, which facilitates the diagnosis of ultrasound images and the reporting of a diagnosis. When images are viewed on a new terminal or display screen, they are often not viewed under the same conditions as they were on the ultrasound system which acquired the images, causing subtle anatomic differences to appear differently. The review workstation or terminal may be in a more dimly or brightly lighted room, for instance, which will affect the appearance of the images in other environments. Different display screens will cause subtle image differences, as will the image file size and image compression which may be used to archive images. The physician could go through an adjustment procedure to optimize the images on the review terminal (e.g., GSDF) but this is usually not done due to its complexity and the time involved in evaluating different display options. Many doctors simply accept the factory default settings on their terminals and settle for sub-optimal images. Accordingly there is a need to simplify the optimization of a workstation, terminal or display screen for the optimal viewing of diagnostic ultrasound images which have been exported from the acquiring ultrasound system.

In accordance with the principles of the present invention, a diagnostic ultrasound system has a setup procedure that optimizes images for display on remote workstations, terminals, and display screens. The ultrasound system enables a user to select one ultrasound image acquired on the ultrasound system which is exported to a remote display terminal with a number of different display settings applied to the image. A user on the remote display terminal views a gallery of the same image with different display settings such as different display gamma correction, file sizes, brightness and/or contrast. The user then selects the image from the gallery with the best appearance on the remote terminal and the display parameters of the selected image are stored on the ultrasound system. Each time a new image or images are exported to the terminal, they are thereafter sent with the selected display settings, assuring that they will be remotely displayed as the remote user desires. Should the remote user have a change of mind or a new display with different characteristics be installed, the process can repeated to update the display parameters applied to images exported to the remote terminal.

In the drawings:

FIG. 1 illustrates in block diagram form an ultrasound system constructed in accordance with the principles of the present invention.

FIG. 2 illustrates an ultrasound system networked with a PACS system.

FIGS. 3a-3f illustrate display screens for setting up an ultrasound system on a network with user preferences for exported images.

FIG. 4 illustrates a method for setting up and exporting a gallery of images with different display settings to a remote terminal.

FIG. 5 illustrates a gallery of images with different display settings which are presented to a user for selection of the best image.

Referring first to FIG. 1 an ultrasonic diagnostic imaging system constructed in accordance with the principles of the present invention is shown in block diagram form. An ultrasound probe 112 includes an array 114 of ultrasonic transducers that transmit and receive ultrasound signals. The

array may be a one dimensional linear or curved array for two dimensional imaging, or may be a two dimensional matrix of transducer elements for electronic beam steering in three dimensions. Three dimensional image data sets and images are preferably acquired using a two dimensional array transducer. Three dimensional images may also be acquired with a mechanically swept one dimensional array probe. The ultrasonic transducers in the array **114** transmit ultrasonic energy and receive echoes returned in response to this transmission. A transmit/receive ("T/R") switch **22** is coupled to the ultrasonic transducers in the array **114** and switches between the transmit and receive phases of pulse-echo imaging. The times at which the transducer array is activated to transmit signals may be synchronized to an internal system clock (not shown), or may be synchronized to a bodily function such as the heart cycle, for which a heart cycle waveform is provided by an ECG device **26**. When the heartbeat is at the desired phase of its cycle as determined by the waveform provided by ECG device **26**, the probe is commanded to acquire an ultrasonic image. The frequency and bandwidth of the ultrasonic energy transmitted by the transducer array is controlled by control signals generated by a central controller **28**.

Echoes from the transmitted ultrasonic energy are received by the transducers of the array **114**, which generate echo signals that are coupled through the T/R switch **22** and digitized by analog to digital ("A/D") converters **30** when the system uses a digital beamformer. Analog beamformers may also be used. The A/D converters **30** sample the received echo signals at a sampling frequency controlled by a signal  $f_s$  generated by the central controller **28**. The desired sampling rate dictated by sampling theory is at least twice the highest frequency of the received passband, and might be on the order of at least 30-40 MHz. Sampling rates higher than the minimum requirement are also desirable.

The echo signal samples from the individual transducers of the array **114** are delayed and summed by a beamformer **32** to form coherent echo signals. For 3D imaging with a two dimensional array, it is preferable to partition the beamformer between a microbeamformer located in the probe and the main beamformer in the system mainframe as described in U.S. Pat. No. 6,013,032 (Savord) and U.S. Pat. No. 6,375,617 (Fraser). The digital coherent echo signals are then filtered by a digital filter **34**. In the illustrated system the transmit frequency and the receiver frequency are individually controlled so that the beamformer **32** is free to receive a band of frequencies which is different from that of the transmitted band such as a harmonic frequency band. The digital filter **34** bandpass filters the signals, and can also shift the frequency band to a lower or baseband frequency range. The digital filter could be a filter of the type disclosed in U.S. Pat. No. 5,833,613, for example. Filtered echo signals from tissue are coupled from the digital filter **34** to a B mode processor **36** for conventional B mode processing.

Filtered echo signals of a contrast agent, such as microbubbles, are coupled to a contrast signal processor **38**. Contrast agents are often used to more clearly delineate the endocardial wall in relation to contrast agent in the blood pool of the heart chamber, or to perform perfusion studies of the microvasculature of the myocardium as described in U.S. Pat. No. 6,692,438 for example. The contrast signal processor **38** preferably separates echoes returned from harmonic contrast agents by the pulse inversion technique, in which echoes resulting from the transmission of multiple pulses to an image location are combined to cancel fundamental signal components and enhance harmonic compo-

ponents. A preferred pulse inversion technique is described in U.S. Pat. No. 6,186,950, for instance.

The filtered echo signals from the digital filter **34** are also coupled to a Doppler processor **40** for conventional Doppler processing to produce velocity and power Doppler signals. The output signals from these processors may be displayed as planar images, and are also coupled to a 3D image processor **42** for the rendering of three dimensional images, which are stored in a 3D image memory **44**. Three dimensional rendering may be performed as described in U.S. Pat. No. 5,720,291, and in U.S. Pat. Nos. 5,474,073 and 5,485,842, all of which are incorporated herein by reference.

The signals from the contrast signal processor **38**, the B mode processor **36** and the Doppler processor **40**, and the three dimensional image signals from the 3D image memory **44** are coupled to a Cineloop® memory **48**, which stores image data for each of a large number of ultrasonic images. The image data are preferably stored in the Cineloop memory **48** in sets, with each set of image data corresponding to an image obtained at a respective time. The image data in a data set can be used to display a parametric image showing tissue perfusion at a respective time during the heartbeat. The sets of image data stored in the Cineloop memory **48** may also be stored in a permanent memory device such as a disk drive or digital video recorder for later analysis. The images in the Cineloop memory are displayed on a display **52**.

When a sonographer begins a particular ultrasound exam the sonographer will generally start by selecting the appropriate probe for the exam, such as a phased array probe for a cardiac exam or a curved linear array for an abdominal or OB exam. The sonographer may then set up and adjust all the imaging parameters for the exam by adjusting the switches and controls on the system control panel **150**. Generally, however, the sonographer will configure the system by calling up the set of standard or previously customized parameters for the type of exam being commenced. These preset parameters are stored in a configuration data memory **152** and are applied to the central controller **28** when selected by the sonographer. The central controller then uses the imaging parameters, as adjusted by the sonographer, to set up and conduct the imaging procedure selected by the sonographer.

In larger hospitals and clinics the ultrasound system is generally connected to a network over which ultrasound images can be communicated. A network interface **54** enables the ultrasound system to communicate over the network and is coupled to a network connection in the hospital or clinic. A typical network with a PACS system is shown in FIG. 2. In FIG. 2, four ultrasound systems **102-106**, a PACS image workstation **244**, and a PACS network server **242** are connected in a local area network as indicated by LAN **240**. The LAN **240** may be wired or wireless and may include both Ethernet hub systems and multi-switch, multi-layered networks. The network server **242** for a PACS system will have extended storage **234** for retention of a large volume of ultrasound images and reports produced by the network's ultrasound systems and image review stations. A user at the image workstation **244** can access the network server and individual active ultrasound systems of the network, or interact over the Internet with other externally accessible networks and devices.

In accordance with the principles of the present invention the ultrasound system of FIG. 1 is configured to export ultrasound images for viewing on a workstation or terminal on a network by use of an export configuration wizard illustrated in FIGS. 3a-3f. The starting screen of FIG. 3a

informs the user that the wizard will guide them through the selection of various export configuration choices for an optimum configuration. The starting screen presents four topics for configuration. For an initial configuration all four topics are used. If the user wants to adjust a configuration that has been implemented previously, the user is given the choice of selecting only the topic(s) to be modified. The subsequent drawings illustrate an initial configuration setup.

When the user clicks on the Next button of the starting screen the Network Configuration screen is presented as shown in FIG. 3*b*. On this screen the user can enter the identification of the network server. The next line on this screen allows the user to specify whether the DHCP (dynamic host configuration protocol) is being used, whether the ultrasound system will have a fixed IP address on the network or a variable (dynamic) IP address assigned by the host server. If the ultrasound system has a fixed IP address it is entered on the next line.

The user clicks the Next button and the PACs Configuration screen appears as shown in FIG. 3*c*. Here the user can select a PACS system from a pulldown list that is on the network and already identified by the wizard. Alternatively the user can click the Custom PACs Configuration radio button and is presented with a screen for entry of data that defines a custom PACS configuration. The user clicks the Next button and is presented with the FIG. 3*d* screen.

On the Image Quality and File Size Selection screen of FIG. 3*d* the user defines one of the parameters that affects how images exported from the ultrasound system appear on the screen of a workstation or terminal on the network. The PACS system or other storage device may store ultrasound images with a predetermined amount of compression or a file size limit. The size of the image file is directly related to the perceived image quality since finer detail can be shown in an image of a larger file size. In this example the user drags a slider 62 horizontally to set the desired image quality. An arrow above the File Size graphic moves correspondingly, showing the user the file size recommended for the desired image quality. The user will generally balance the desired image quality and file size to obtain the highest quality images within the bounds of the permitted size of images archived on the PACS system. The user clicks the Next button and is presented with the screen of FIG. 3*e*.

The Image Acquisition & Review Environment screen enables a user to set another parameter that affects how images acquired by the ultrasound system will appear on the remote terminal. The patient scanning room may be only dimly lighted and consequently the user may employ low brightness and contrast settings to view the ultrasound images as they are acquired. The physician reading the images may be viewing them in a brightly lighted room, which means that the view settings on the ultrasound system will not be suited to the ambient lighting conditions of the reading room. Or, the reverse may be true. With the screen of FIG. 3*e* the user can adjust slider 64 to indicate the ambient lighting conditions in the scanning room as low, high, or intermediate. The user can also check the GSDF (grayscale standard display function) box if the display at the remote terminal has this DICOM calibrated display function, in which case further display optimization is not necessary.

After the user has adjusted the last set of display parameters the user is presented with the closing screen of FIG. 3*f*. If the user has finished specifying the PACS and image export parameters the user can click on the Finish button to conclude the export configuration process. If the user has encountered a problem or has a question, the user can click

on the question mark symbol to request technical assistance in completing the configuration process.

With the export parameters and network protocols thus set, the user now prepares an export of images that will be displayed with different display parameters as exemplified by the export screens of FIG. 4. In this set of screens, identified as the Export IQ Wizard, the user is guided through the acquisition of an ultrasound image and its export with different processing for viewing and selection on a remote terminal. The first screen 70 instructs the user to prepare the ultrasound system to scan an image under the condition generally preferred by the user, such as in an appropriately lighted room. If the display at the remote terminal is DICOM GSDF calibrated, this compensation procedure is not needed, however. The user will then click the DICOM GSDF Enabled radio button and proceed to Finish this compensation procedure, as indicated by screen 72.

When the user clicks the Continue button on screen 70 to proceed with the compensation procedure, the user is shown screen 74. This screen instructs the user to acquire an ultrasound image with the ultrasound system. The user can do this by scanning a patient at this time, in which case the user will click the Continue button on screen 74 and will scan a subject. After the user has acquired a satisfactory image the user presses Acquire 1 on the ultrasound system control panel 150. Alternatively, the user can select a previously acquired satisfactory image from the image storage on the ultrasound system. Again, the user indicates that a satisfactory image has been obtained by pressing Acquire 1 on the ultrasound system control panel 150.

With the basic compensation image identified, the user selects a destination to which compensation selection images are to be exported using screen 76. In this example the user has selected Archive Server 1, a PACS image storage device on the network where the images are stored with the image processing employed by the PACS system. Screen 76 gives examples of different export destinations including one called PC Media for ultrasound systems not connected to a reading station by a network. If this radio button is selected the screen 78 appears to instruct the user to insert media into the ultrasound system such as a portable flash drive. The images are then transferred to the flash drive which can be carried to the reading workstation for the compensation setup. In this example the user has selected Archive Server 1 and a set of compensation images such as that of FIG. 5 is sent to the Archive Server 1 PACS system. Screen 80 is then displayed to the user, instructing the user to view the compensation images on the PACS system display terminal and select the image that best represents the basic image acquired by or selected on the ultrasound system.

FIG. 5 is an example of a set of compensation images 200 that are exported to the PACS system and viewed on a review station on the PACS system such as terminal 244 in FIG. 2. Each of the twenty-five compensation images has been processed by the controller 28 or contains slightly different display parameters that will affect its appearance on a display screen. For instance, each of the twenty-five images can be processed by a slightly different display device gamma correction characteristic. Or each image will have a slightly different brightness or contrast to compensate for different ambient lighting conditions. The user views all twenty-five images simultaneously on the remote terminal display screen and selects the one which appears the best on that display screen. The user can click on the up and down arrows in the selection box 210 at the bottom of the screen

to select the number of the best image. In this example the user has selected image number 13. Alternatively the user can click on an image to select it, such as clicking on image 202 to select that image as the best compensated image. When the user makes the selection the identity of the selection is sent back to the ultrasound system where the display parameters of the selected image are stored in a lookup table in the configuration data memory 152 of the system in association with the export destination device, Archive Server 1 in this example. Thereafter, whenever images are exported from the ultrasound system to Archive Server 1, the display parameters stored in the lookup table in memory for that PACS system are applied to the images prior to export so that they are properly compensated to appear on the PACS terminal just as they appeared on the ultrasound system. A reviewer on the PACS workstation will then be viewing an exported image with the same image quality and characteristics as seen by the sonographer who acquired the image.

Screen 80 of FIG. 4 also gives the user the ability to select the desired image from the screen on the ultrasound system. The user can make the selection on screen 80, then click the Finish button to conclude the image export compensation process.

A PACS system may have multiple review stations or terminals on the system and each may have a different display characteristic. In that event, the foregoing compensation process may be performed for each display device of each station or terminal. The ultrasound system will then use the correspondingly identified display station when exporting images for display on one of the terminals.

A review station or terminal can also be replaced or modified with a different display screen or used by a clinician with different viewing preferences, requiring that the compensation be performed again for the new or different display device or reviewer. In that event, the Export IQ Wizard of FIG. 4 can be called up on the ultrasound system to send a new set of compensation screens to the terminal and the compensation selection process performed again and new display parameters for the terminal stored in the configuration data memory 152. Alternatively, the clinician at the review station can send a query to the ultrasound system, requesting transmission of another set of compensation images. The user of the remote terminal can thereby adjust or update the display parameters of images exported from the ultrasound system without interrupting the workflow of the sonographer who is using the ultrasound system.

The present invention has applicability in other medical imaging modalities, particularly in the use of "secondary captures," image information which is derived from a primary diagnostic image. For example, an MRI image of the body may show an invasive instrument such as a biopsy needle which a clinician wants to view in well defined resolution. The optimization technique of the present invention can be used to optimize the displayed images for optimal viewing of this secondary capture, the needle in the MRI image.

What is claimed is:

1. An ultrasound system, comprising:
  - a processor configured to produce a plurality of versions of an ultrasound image of a first view such that each version of the ultrasound image of the first view has a different display appearance when displayed;
  - a data storage device configured to, in response to a user selection of at least one version of the ultrasound image of the first view, store a parameter for the at least one

version of the ultrasound image of the first view selected by the user, wherein the parameter is further associated with an identifier of a remote terminal where the user selection input was entered; and  
 an export processor configured to export a subsequent ultrasound image to the remote terminal based at least in part on the parameter.

2. The ultrasound system of claim 1, wherein the remote terminal comprises a display screen configured to display the plurality of versions of the ultrasound image of the first view simultaneously.

3. The ultrasound system of claim 1, wherein the parameter comprises a display device gamma characteristic, image brightness or image contrast.

4. The ultrasound system of claim 3, wherein the remote terminal comprises a PACS system or PACS system image archive.

5. The ultrasound system of claim 3, wherein the remote terminal comprises one of a plurality of workstations of a PACS system.

6. The ultrasound system of claim 1, further comprising a network input and a network output configured to connect the ultrasound system and the remote terminal.

7. The ultrasound system of claim 1, wherein the remote terminal and the ultrasound system are not on a common network, wherein the plurality of versions of the image are exported to the remote terminal on portable media.

8. The ultrasound system of claim 1, further comprising an input device by which ambient light condition data can be input into the ultrasound system, wherein the image processor is configured to produce the plurality of versions of the image for export based at least in part on the ambient light condition data.

9. The ultrasound system of claim 1, further comprising an input device by which image file size data is input into the ultrasound system,

wherein the image processor is configured to produce the plurality of versions of the image for export based at least in part on the image file size data.

10. The ultrasound system of claim 9, wherein the image file size comprises the file size of images stored on a network image archive.

11. The ultrasound system of claim 1, further comprising an input device by which image quality data is input into the ultrasound system,

wherein the image processor is configured to produce the plurality of versions of the image for export based at least in part on the image quality data.

12. The ultrasound system of claim 1, wherein the data storage device is further configured to store the parameter for the version of the selected image in lookup table form.

13. The ultrasound system of claim 1, wherein the processor is configured to produce a plurality of versions of the image for export from an input initiated from the ultrasound system.

14. The ultrasound system of claim 1, wherein the processor is configured to produce a plurality of versions of the ultrasound image for export from an input initiated from the remote terminal.

15. The ultrasound system of claim 1, wherein the data storage device is configured to store a plurality of parameters, each in association with an identifier of a different remote terminal, wherein the export processor is configured to export images based at least in part on the identifier of the remote terminal.

专利名称(译)	用于远程显示终端的超声图像显示设置		
公开(公告)号	<a href="#">US10372399</a>	公开(公告)日	2019-08-06
申请号	US15/871164	申请日	2018-01-15
[标]申请(专利权)人(译)	皇家飞利浦电子股份有限公司		
申请(专利权)人(译)	皇家飞利浦N.V.		
当前申请(专利权)人(译)	皇家飞利浦N.V.		
[标]发明人	RUST DAVID THIELE KARL ERHARD BRADLEY KEVIN CANFIELD EARL M		
发明人	RUST, DAVID THIELE, KARL ERHARD BRADLEY, KEVIN CANFIELD, EARL M.		
IPC分类号	A61B8/00 G01S7/00 G16H40/40 G06F3/14 G01S7/52 G09G5/14 G16H30/40 G16H30/20 G16H10/60		
CPC分类号	G06F3/1423 A61B8/565 G01S7/003 G01S7/52053 G01S7/52084 G06F3/1454 G09G5/14 G16H30/20 G16H30/40 G16H40/40 A61B8/463 G09G2380/08 A61B8/464 F04C2270/041 G09G2354/00 G06F19/321 G16H40/67 A61B8/00 G01S7/52 G16Z99/00		
优先权	PCT/IB2013/053788 2013-05-10 WO 61/650241 2012-05-22 US		
其他公开文献	US20180136896A1		
外部链接	<a href="#">Espacenet</a>		

摘要(译)

超声系统使得能够简化远程终端的设置，以显示由超声系统获取的超声图像。由超声系统获取的图像由用于不同观看条件或设备的显示参数处理或与显示参数一起处理，例如显示器伽马校正，环境照明或图像质量。将具有略微不同的显示外观的图像的版本导出到远程终端，其中观看者可以同时查看所有图像版本。观看者选择最佳图像，并且所选图像的显示特性用于随后从超声系统输出到远程终端的图像。

