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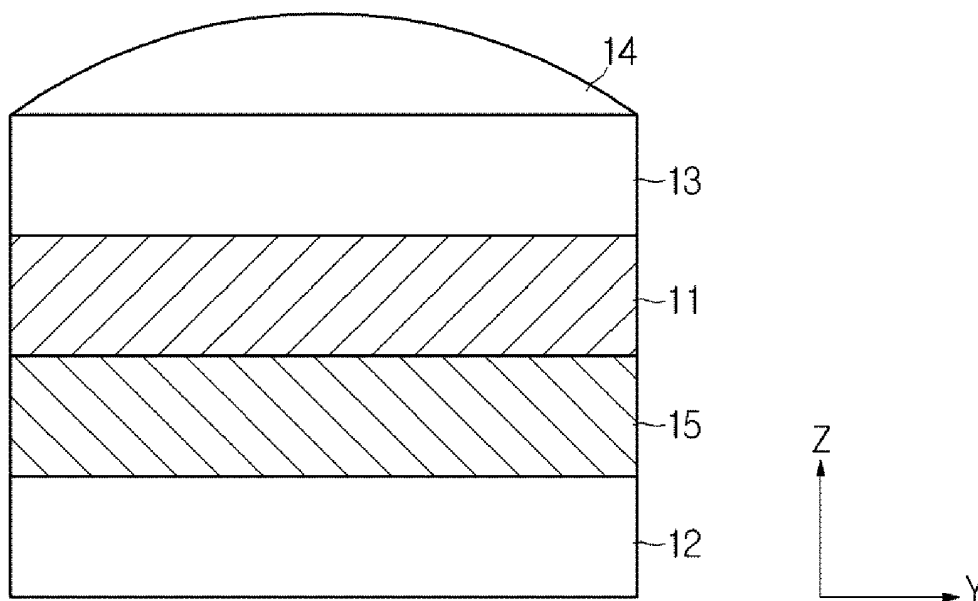
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(54) **Ultrasonic probe and ultrasonic imaging apparatus having the same**

(57) Provided are an ultrasonic probe that controls temperature of a piezoelectric layer using a thermoelectric element and an ultrasonic imaging apparatus having the same. The ultrasonic probe includes: the piezoelectric layer that vibrates and generates ultrasonic waves if

a current is supplied to the piezoelectric layer; and a thermoelectric element that contacts one surface of the piezoelectric layer and controls the temperature of the piezoelectric layer if a current is supplied to the thermoelectric element.

FIG. 3



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Description

BACKGROUND

1. Field

[0001] Embodiments of the present invention relate to an ultrasonic probe for generating an image of an inside of a subject using ultrasonic waves and an ultrasonic imaging apparatus having the same.

2. Description of the Related Art

[0002] Ultrasonic diagnosis apparatuses are apparatuses that radiate ultrasonic signals onto a target part of a body from a body surface of the subject and obtain a tomogram of a soft tissue or an image of a blood flow of the soft tissue using information regarding reflected ultrasonic signals (ultrasonic echo signals) in a noninvasive manner.

[0003] In comparison with other image diagnosis apparatuses, such as X-ray diagnosis apparatuses, X-ray computerized tomography (CT) scanners, magnetic resonance imaging (MRI) apparatuses, and nuclear medicine apparatuses, ultrasonic diagnosis apparatuses are small-sized and cheap, can be displayed in real time and have high safety due to lack of radiation exposure. Thus, ultrasonic diagnosis apparatuses are widely used in heart, abdominal, urinary, and ob-gyn diagnoses.

[0004] Meanwhile, an ultrasonic probe that radiates ultrasonic waves may include a transducer installed in the ultrasonic probe. An inner side of the ultrasonic probe is required to be maintained at an appropriate temperature so that the transducer operates normally.

SUMMARY

[0005] Therefore, it is an aspect of the present invention to provide an ultrasonic probe that controls temperature of a piezoelectric layer using a thermoelectric element, and an ultrasonic imaging apparatus having the same.

[0006] Additional aspects of the invention will be set forth in part in the description which follows and, in part, will be obvious from the description, or may be learned by practice of the invention.

[0007] In accordance with one aspect of the present invention, an ultrasonic probe includes: a piezoelectric layer that vibrates and generates ultrasonic waves if a current is supplied to the piezoelectric layer; and a thermoelectric element that contacts one surface of the piezoelectric layer and controls temperature of the piezoelectric layer if a current is supplied to the thermoelectric element.

[0008] The thermoelectric element may include: a heat dissipation plate that is disposed on one surface of the thermoelectric element and dissipates heat toward a contact surface between the piezoelectric layer and the ther-

moelectric element; and a heat absorption plate that is disposed at an opposite side to the heat dissipation plate and absorbs heat of the contact surface.

[0009] The thermoelectric element may contact the piezoelectric layer through the heat dissipation plate and may heat the piezoelectric layer.

[0010] The thermoelectric element may contact the piezoelectric layer through the heat absorption plate and may cool the piezoelectric layer.

[0011] The piezoelectric layer and the thermoelectric element may share a signal electrode through which a current is supplied to the piezoelectric layer and the thermoelectric element, respectively.

[0012] The piezoelectric layer and the thermoelectric element may share a ground electrode.

[0013] When the piezoelectric layer includes one or more piezoelectric channels, the thermoelectric element may include one or more thermoelectric channels corresponding to the one or more piezoelectric channels.

[0014] In accordance with another aspect of the present invention, an ultrasonic probe includes: a piezoelectric layer that vibrates and generates ultrasonic waves if a current is supplied to the piezoelectric layer; an application specific integrated circuit (ASIC) that transfers the current to the piezoelectric layer; and a thermoelectric element that contacts one surface of the ASIC and controls temperature of the piezoelectric layer if a current is supplied to the thermoelectric element.

[0015] The thermoelectric element may include: a heat dissipation plate that is disposed on one surface of the thermoelectric element and dissipates heat toward a contact surface between the piezoelectric layer and the thermoelectric element; and a heat absorption plate that is disposed at an opposite side to the heat dissipation plate and absorbs heat of the contact surface.

[0016] The piezoelectric layer and the thermoelectric element may share a signal electrode through which a current is supplied to the piezoelectric layer and the thermoelectric element, respectively.

[0017] The piezoelectric layer and the thermoelectric element may share a ground electrode.

[0018] In accordance with still another aspect of the present invention, an ultrasonic imaging apparatus includes: an ultrasonic probe including a piezoelectric layer that vibrates and generates ultrasonic waves, a thermoelectric element that contacts one surface of the piezoelectric layer and controls temperature of the piezoelectric layer according to a supplied current, and a temperature sensor that senses the temperature of the piezoelectric layer; and a controller that controls the supplied current based on the sensed temperature.

[0019] In accordance with yet still another aspect of the present invention, an ultrasonic imaging apparatus includes: an ultrasonic probe including a piezoelectric layer that vibrates and generates ultrasonic waves, an application specific integrated circuit (ASIC) that transfers a current to the piezoelectric layer, a thermoelectric element that contacts one surface of the ASIC and con-

trols temperature of the piezoelectric layer according to the supplied current, and a temperature sensor that senses the temperature of the piezoelectric layer; and a controller that controls the supplied current based on the sensed temperature.

BRIEF DESCRIPTION OF THE DRAWINGS

[0020] These and/or other aspects of the invention will become apparent and more readily appreciated from the following description of the embodiments, taken in conjunction with the accompanying drawings of which:

FIG. 1 is a perspective view of an ultrasonic imaging apparatus in accordance with an embodiment of the present invention;

FIG. 2A is a perspective of an ultrasonic probe according to the related art, and FIG. 2B is an exploded perspective view of the ultrasonic probe illustrated in FIG. 2A;

FIG. 3 illustrates an ultrasonic probe including a thermoelectric element, in accordance with an embodiment of the present invention;

FIGS. 4A through 4C illustrate ultrasonic probes including a signal electrode and a ground electrode, in accordance with other embodiments of the present invention;

FIGS. 5A through 5E illustrate ultrasonic probes including an application specific integrated circuit (ASIC), in accordance with various embodiments of the present invention;

FIGS. 6A and 6B illustrate ultrasonic probes in which a piezoelectric layer is diced, in accordance with other embodiments of the present invention; and

FIG. 7 is a control block diagram of an ultrasonic imaging apparatus including the ultrasonic probe in which the thermoelectric element is disposed, in accordance with an embodiment of the present invention.

DETAILED DESCRIPTION

[0021] Reference will now be made in detail to the embodiments of the present invention, examples of which are illustrated in the accompanying drawings, wherein like reference numerals refer to like elements throughout.

[0022] FIG. 1 is a perspective view of an ultrasonic imaging apparatus in accordance with an embodiment of the present invention. As illustrated in FIG. 1, the ultrasonic imaging apparatus may include a body 100, an ultrasonic probe 110, an input unit 150, and a display 160. In this case, the display 160 may include a main display 161 and a subdisplay 162.

[0023] One or more female connectors 145 may be provided at one side of the body 100. A male connector 140 connected to a cable 130 may be physically coupled to the female connector 145.

[0024] A plurality of casters (not shown) for mobility of

the ultrasonic imaging apparatus may be provided at a lower portion of the body 100. The plurality of casters (not shown) may fix the ultrasonic imaging apparatus at a particular place or may move the ultrasonic imaging apparatus in a particular direction.

[0025] The ultrasonic probe 110 that contacts a body surface of a subject may transmit and receive ultrasonic waves. One end of the cable 130 may be connected to the ultrasonic probe 110, and the male connector 140 may be connected to the other end of the cable 130. The male connector 140 connected to the other end of the cable 130 may be physically coupled to the female connector 145 of the body 100.

[0026] Instructions relating to an operation of the ultrasonic imaging apparatus may be input to the input unit 150. For example, mode selection instructions, such as an amplitude mode (A-mode), a brightness mode (B-mode), and a motion mode (M-mode), or ultrasonic diagnosis starting instructions may be input to the input unit 150. The instructions input through the input unit 150 may be transmitted to the body 100 through wired or wireless communication.

[0027] The input unit 150 may include at least one of a keyboard, a foot switch, and a foot pedal, for example.

The keyboard may be implemented with hardware and may be placed at an upper portion of the body 100. The keyboard may include at least one of a switch, a key, a joystick, and a trackball. Alternatively, the keyboard may be implemented with software, like a graphic user interface. In this case, the keyboard may be displayed on the subdisplay 162 or the main display 161. The foot switch or the foot pedal may be disposed at the lower portion of the body 100, and a manipulator may control the operation of the ultrasonic imaging apparatus using the foot pedal.

[0028] An ultrasonic probe holder 120 for holding the ultrasonic probe 110 may be disposed around the input unit 150. One or more ultrasonic probe holders 120 may be provided. When an inspector does not use the ultrasonic imaging apparatus, the ultrasonic probe 110 may be held by and kept in the ultrasonic probe holder 120.

[0029] The subdisplay 162 may be disposed on the body 100. FIG. 1 illustrates a case that the subdisplay 162 is disposed at an upper portion of the input unit 150.

The subdisplay 162 may display an application relating to the operation of the ultrasonic imaging apparatus. For example, the subdisplay 162 may display a menu or information required for ultrasonic diagnosis. The subdisplay 162 may be implemented with a cathode ray tube (CRT) or a liquid crystal display (LCD), for example.

[0030] The main display 161 may be disposed at the body 100. FIG. 1 illustrates a case that the main display 161 is disposed at an upper portion of the subdisplay 162. The main display 161 may display an ultrasonic image obtained during an ultrasonic diagnosis procedure. The main display 161 may be implemented with a CRT or an LCD, like in the subdisplay 162. Although FIG. 1 illustrates a case that the main display 161 is coupled to

the body 100, the main display 161 may be implemented to be detachable from the body 100.

[0031] FIG. 1 illustrates a case that both the main display 161 and the subdisplay 162 are provided at the ultrasonic imaging apparatus. However, the subdisplay 162 may be omitted, as needed. In this case, the application or menu displayed on the subdisplay 162 may be displayed on the main display 161.

[0032] Until now, a general configuration of the ultrasonic imaging apparatus has been described. Hereinafter, an ultrasonic probe according to the present invention will be described in more detail.

[0033] FIG. 2A is a perspective of an ultrasonic probe according to the related art, and FIG. 2B is an exploded perspective view of the ultrasonic probe illustrated in FIG. 2A.

[0034] An ultrasonic probe 110 according to the related art may include a piezoelectric layer 11, a matching layer 13 disposed on a top surface of the piezoelectric layer 11, a lens 14 installed at a top surface of the matching layer 13, and a backing layer 12 disposed on a bottom surface of the piezoelectric layer 11.

[0035] The effects that, if mechanical pressure is applied to a predetermined material, a voltage is generated and if a voltage is applied to the predetermined material, mechanical deformation occurs, are referred to as a piezoelectric effect and an inverse piezoelectric effect, and a material having these effects is referred to as a piezoelectric material. That is, the piezoelectric material is a material that transforms electric energy into mechanical vibration energy or vice versa.

[0036] The ultrasonic probe 110 of FIG. 1 includes the piezoelectric layer 11 that transforms a received electrical signal into mechanical vibration so as to generate ultrasonic waves.

[0037] The piezoelectric material that constitutes the piezoelectric layer 11 may include a ceramic of lead zirconate titanate (PZT), a PZMT monocrystal formed of a solid solution of lead magnesium niobate (PMN) and lead titanate (PT), or a PZNT monocrystal formed of a solid solution of lead zinc niobate (PZN) and PT.

[0038] The backing layer 12 is mounted on the bottom surface of the piezoelectric layer 11, absorbs the ultrasonic waves generated in the piezoelectric layer 11, and blocks the ultrasonic waves that proceed toward the bottom surface of the piezoelectric layer 11, thereby preventing distortion of an image. The backing layer 12 may be manufactured as a plurality of layers so as to improve an attenuation or blocking effect of the ultrasonic waves.

[0039] The matching layer 13 is disposed on the top surface of the piezoelectric layer 11 and reduces a difference in sound impedance between the piezoelectric layer 11 and the subject so that ultrasonic waves generated in the piezoelectric layer 11 can be effectively transferred to the subject. The matching layer 13 may be formed to have one or more layers.

[0040] The matching layer 13 may be divided into a plurality of units having predetermined widths together

with the piezoelectric layer 11 through a dicing process.

[0041] Although not shown, a protective layer may be disposed on the top surface of the matching layer 13. The protective layer may prevent outflow of high frequency components that may be generated in the piezoelectric layer 11 and may block inflow of external high frequency signals. Also, the protective layer may protect internal parts of the ultrasonic probe from water or medicine used in disinfection by coating or depositing a conductive material on the surface of a film having moisture tolerance and chemical resistance.

[0042] The lens 14 is installed at the top surface of the matching layer 13. The lens 14 may have a convex shape in a radiation direction of the ultrasonic waves so as to focus the ultrasonic waves, and when sound speed is slower than the human body, the lens 14 may be implemented with a concave shape.

[0043] Meanwhile, all parts of vibration of the piezoelectric layer 11 are not transformed into ultrasonic waves but parts thereof are converted into heat, and thus a sound loss occurs. Heat generated in this way may increase an internal temperature of the ultrasonic probe 110 to 40°C or higher. Since the high-temperature ultrasonic probe 110 directly contacts a skin, a patient's health may be under threat. If heat generated in the piezoelectric layer 11 is not properly dissipated, performance of the ultrasonic probe 110 may be adversely affected. In particular, a depolarization phenomenon may occur in the piezoelectric material that constitutes the piezoelectric layer 11 in a high-temperature environment. This may cause performance of the piezoelectric layer 11 to be degraded.

[0044] When the ultrasonic probe 110 is in a high-temperature state and in an extremely low temperature environment, performance degradation may occur. Thus, the temperature of the ultrasonic probe 110, in detail, the temperature of the piezoelectric layer 11 is required to be uniformly maintained regardless of a peripheral environment.

[0045] FIG. 3 illustrates an ultrasonic probe including a thermoelectric element, in accordance with an embodiment of the present invention.

[0046] As illustrated in FIG. 3, a thermoelectric element 15 may contact one surface of the piezoelectric layer 11 so as to control the temperature of the piezoelectric layer 11. Here, the thermoelectric element 15 is an element that uses the peltier effect that one terminal causes a heat absorption reaction and the other terminal causes a heat dissipation reaction according to a direction of a current if ends of different types of metals are connected to each other and a current flows through the connected metal ends.

[0047] In an embodiment of the thermoelectric element 15, the thermoelectric element 15 may include a heat dissipation plate that is disposed at one surface of the thermoelectric element 15 and dissipates heat, and a heat absorption plate that is disposed at an opposite side to the heat dissipation plate and absorbs heat.

[0048] In this case, the used thermoelectric element 15 may be a thin film type thermoelectric element 15. The thickness of the thermoelectric element 15 may be several tens of micrometers (um) to several hundreds of micrometers (um). The thinner the thermoelectric element 15, the less effect on sound performance of the piezoelectric layer 11, but performance of the thermoelectric element 15 is degraded. Thus, an appropriate thickness of the thermoelectric element 15 may be determined according to situations and may be applied to the ultrasonic probe 110.

[0049] If the thermoelectric element 15 contacts one surface of the piezoelectric layer 11 through the heat dissipation plate, the heat dissipation plate may dissipate heat and may heat the piezoelectric layer 11. In contrast, if the thermoelectric element 15 contacts one surface of the piezoelectric layer 11 through the heat absorption plate, the heat absorption plate may absorb heat generated in the piezoelectric layer 11 and may cool the piezoelectric layer 11.

[0050] FIG. 3 illustrates the ultrasonic probe 110 in which the thermoelectric element 15 contacts a bottom surface of the piezoelectric layer 11, in accordance with an embodiment of the present invention. The piezoelectric layer 11 and the thermoelectric element 15 may make surface contact with each other and may be configured such that conduction of heat may be easily performed. In this case, a thermal compound may be used to improve the effects of surface contact.

[0051] When ultrasonic diagnosis is performed in an extremely low-temperature environment, the piezoelectric layer 11 needs to be heated for a normal operation of the ultrasonic probe 110. To this end, the heat dissipation plate may be disposed on a top surface of the thermoelectric element 15, i.e., on a surface that makes surface contact with the piezoelectric layer 11. Heat generated in the heat dissipation plate provided in this way may be transferred to the piezoelectric layer 11, and the piezoelectric layer 11 to which heat is transferred, may be maintained at a uniform temperature and may generate ultrasonic waves normally.

[0052] Alternatively, an internal temperature of the ultrasonic probe 110 may be increased due to heat generated due to vibration of the piezoelectric layer 11. If heat generated in this way is not dissipated, normal ultrasonic diagnosis becomes difficult. To this end, the heat absorption plate may be disposed on the top surface of the thermoelectric element 15, i.e., on a surface that makes surface contact with the piezoelectric layer 11. Heat generated in the piezoelectric layer 11 is absorbed by the heat absorption plate so that the piezoelectric layer 11 may be cooled and the internal temperature of the ultrasonic probe 110 may be prevented from being increased.

[0053] As a result, the piezoelectric layer 11 and the thermoelectric element 15 make surface contact with each other so that the piezoelectric layer 11 can be maintained at a uniform temperature and the ultrasonic probe

110 can operate normally.

[0054] FIGS. 4A through 4C illustrate ultrasonic probes including a signal electrode and a ground electrode, in accordance with embodiments of the present invention. Arrows in FIGS. 4A through 4C mean a direction in which a current flows.

[0055] The current may be supplied to the piezoelectric layer 11 so that the piezoelectric layer 11 generates ultrasonic waves. To this end, the piezoelectric layer 11 may include a signal electrode 16a for the piezoelectric layer 11 to which the current is supplied, and a ground electrode 17a for the piezoelectric layer 11 through which the current is discharged. If the current is supplied to the piezoelectric layer 11 via the signal electrode 16a for the piezoelectric layer 11, the piezoelectric layer 11 vibrates and generates ultrasonic waves.

[0056] Since the thermoelectric element 15 generates a temperature difference between both ends of the thermoelectric element 15 due to the peltier effect, a supply of current is required. To this end, the thermoelectric element 15 may include a signal electrode 16b for the thermoelectric element 15 to which a current is supplied, and a ground electrode 17b for the thermoelectric element 15 through which the current is discharged. The thermoelectric element 15 generates a temperature difference between both ends of the thermoelectric element 15 due to the current supplied to the thermoelectric element 15 through the signal electrode 16b, thereby controlling the temperature of the piezoelectric layer 11.

[0057] FIG. 4A illustrates the ultrasonic probe 110 in which the piezoelectric layer 11 and the thermoelectric element 15 make surface contact with each other, i.e., a case that a signal electrode and a ground electrode are disposed on the piezoelectric layer 11 and the thermoelectric element 15, respectively, in accordance with an embodiment of the present invention. In this case, a current is supplied to the piezoelectric layer 11 through the signal electrode 16a for the piezoelectric layer 11, and a current is supplied to the thermoelectric element 15 through the signal electrode 16b for the thermoelectric element 15. Thus, the piezoelectric layer 11 and the thermoelectric element 15 operate due to separate currents.

[0058] FIG. 4B illustrates the ultrasonic probe 110 in which the piezoelectric layer 11 and the thermoelectric element 15 make surface contact with each other, i.e., a case that the piezoelectric layer 11 and the thermoelectric element 15 share a ground electrode, in accordance with another embodiment of the present invention. In this case, a current is supplied to the piezoelectric layer 11 through the signal electrode 16a for the piezoelectric layer 11, and a current is supplied to the thermoelectric element 15 through the signal electrode 16b for the thermoelectric element 15, like in FIG. 4A. However, there is a difference between FIGS. 4A and 4B in that, in FIG. 4B, the current flows to the ground through one ground electrode. Hereinafter, the ground electrode shared by the piezoelectric layer 11 and the thermoelectric element 15 is referred to as a shared ground electrode 17.

[0059] As illustrated in FIG. 4B, if the piezoelectric layer 11 and the thermoelectric element 15 share the ground electrode, only one ground electrode is sufficient. Connection lines connected to the outside are required to be provided in each electrode. If the number of electrodes is reduced, the number of connection lines that accompany with the number of electrodes is also reduced to overcome a limitation in an internal space of the ultrasonic probe 110.

[0060] Also, even when the piezoelectric layer 11 and the thermoelectric element 15 are diced, the risk of generating an electrical short is low. In addition, interference that occurs between a plurality of electrode layers is reduced so that sound performance can be uniformly maintained.

[0061] FIG. 4C illustrates the ultrasonic probe 110 in which the piezoelectric layer 11 and the thermoelectric element 15 make surface contact with each other, i.e., a case that the piezoelectric layer 11 and the thermoelectric element 15 share a ground electrode and a signal electrode, in accordance with still another embodiment of the present invention. Hereinafter, the signal electrode shared by the piezoelectric layer 11 and the thermoelectric element 15 is referred to as a shared signal electrode 16.

[0062] Referring to FIG. 4C, a current may be supplied to the thermoelectric element 15 via the shared signal electrode 16 disposed on a bottom surface of the thermoelectric element 15. A surface of the thermoelectric element 15 on which the shared signal electrode 16 is disposed, may be a heat dissipation plate. When the supplied current flows from the heat dissipation plate to the heat absorption plate, a temperature difference may be generated in both ends of the thermoelectric element 15. As a result, heat generated in the piezoelectric layer 11 is absorbed by the heat absorption plate, and thus the piezoelectric layer 11 may be cooled.

[0063] Also, the current that flows through the heat absorption plate may be transferred to the piezoelectric layer 11 and may vibrate the piezoelectric layer 11. The current may be discharged through the shared ground electrode 17 disposed on a top surface of the piezoelectric layer 11.

[0064] As illustrated in FIG. 4C, if a current is supplied through the shared signal electrode 16, a temperature difference of the thermoelectric element 15 may be generated due to the supplied current, and the piezoelectric layer 11 may be vibrated, and ultrasonic waves may be generated. Unlike in FIG. 4A or 4B in which the piezoelectric layer 11 and the thermoelectric element 15 are controlled due to separate currents, the piezoelectric layer 11 and the thermoelectric element 15 are controlled when one current flows through the piezoelectric layer 11 and the thermoelectric element 15 via the shared signal electrode 16.

[0065] In this way, if the piezoelectric layer 11 and the thermoelectric element 15 share the signal electrode as well as the ground electrode, the number of electrodes

and the number of connection lines that accompany with the number of electrodes are reduced such that there is no problem of the limitation in the internal space of the ultrasonic probe 110.

[0066] Also, even when the piezoelectric layer 11 and the thermoelectric element 15 are diced, there is a low possibility that an electrical short will occur. In addition, interference that occurs between a plurality of electrode layers is reduced so that sound performance is not degraded.

[0067] FIGS. 5A through 5E illustrate ultrasonic probes including an application specific integrated circuit (ASIC), in accordance with various embodiments of the present invention.

[0068] As the configuration of the ultrasonic probe 110 is recently diversified, complexity of an inside of the ultrasonic probe 110 increases. In particular, as an arrangement shape of a transducer device is complicated, the ultrasonic probe 110 may include an application specific integrated circuit (ASIC) so as to control a current supplied to each device. Owing to integration technology using the ASIC, the reliability of the ultrasonic probe 110 and the ultrasonic imaging apparatus can be increased, and complexity of the ultrasonic probe 110 can be decreased, and excellent signal processing efficiency can be obtained.

[0069] In this way, even when the ultrasonic probe 110 includes the ASIC so as to transfer the current to the piezoelectric layer 11, the ultrasonic probe 110 may include the thermoelectric element 15 so as to control the temperature of the piezoelectric layer 11.

[0070] FIGS. 5A through 5C illustrate the ultrasonic probe 110 in which an ASIC 11a makes surface contact with the bottom surface of the piezoelectric layer 11 and the thermoelectric element 15 makes surface contact with a bottom surface of the ASIC 11a, in accordance with various embodiments of the present invention. In this case, since the ASIC 11a controls the supplied current and transfers the current to the piezoelectric layer 11, each embodiment of the ultrasonic probe 110 including the ASIC 11a is subject to a case that the supplied current is transferred to the piezoelectric layer 11 via the ASIC 11a. Arrows of FIGS. 5A through 5E represent a direction in which the current flows.

[0071] FIG. 5A illustrates a case that the piezoelectric layer 11 includes a signal electrode and a ground electrode for the piezoelectric layer 11 and the thermoelectric element 15 includes a signal electrode and a ground electrode for the thermoelectric element 15. The signal electrode 16a for the piezoelectric layer 11 may be disposed on the ASIC 11a, and a current may be supplied to the signal electrode 16a for the piezoelectric layer 11. The current supplied in this way may be controlled by the ASIC 11a and may be transferred to the piezoelectric layer 11, and the piezoelectric layer 11 to which the current is transferred, may vibrate and generate ultrasonic waves. Also, the current is discharged along the ground electrode 17a disposed on the piezoelectric layer 11.

[0072] Meanwhile, the thermoelectric element 15 may include the signal electrode 16b and the ground electrode 17b for the thermoelectric element 15. In FIG. 5A, the signal electrode 16b for the thermoelectric element 15 is disposed on the bottom surface of the thermoelectric element 15. Thus, the bottom surface of the thermoelectric element 15 is a heat dissipation plate. The current supplied along the signal electrode 16b for the thermoelectric element 15 flows from the heat dissipation plate to an opposite site, i.e., to a heat absorption plate and is discharged along the ground electrode 17b for the thermoelectric element 15. In this case, the heat absorption plate absorbs heat generated in the piezoelectric layer 11 via the ASIC 11 a and thus may cool the piezoelectric layer 11.

[0073] Unlike in FIG. 5A, FIG. 5B illustrates a case that the shared ground electrode 17 is disposed. The current supplied along the signal electrode 16a for the piezoelectric layer 11 disposed on the ASIC 11 a vibrates the piezoelectric layer 11 and is discharged along the shared ground electrode 17. Also, the current supplied along the signal electrode 16b for the thermoelectric element 15 generates a temperature difference in both ends of the thermoelectric element 15 and is discharged along the shared ground electrode 17 disposed on the thermoelectric element 15 via the ASIC 11 a.

[0074] When the shared ground electrode 17 is disposed in this way, the number of ground electrodes may be reduced to one, and the number of connection lines that accompany with the number of ground electrodes may be reduced, too. Thus, the limitation in the internal space of the ultrasonic probe 110 can be overcome.

[0075] Also, even when the piezoelectric layer 11 and the thermoelectric element 15 are diced, the risk of generating an electrical short is low. In addition, interference that occurs between a plurality of electrode layers is reduced so that uniform sound performance can be maintained.

[0076] FIG. 5C illustrates a case that the shared signal electrode 16 as well as the shared ground electrode 17 are provided, unlike in FIG. 5B. Since the shared signal electrode 16 is disposed on the bottom surface of the thermoelectric element 15, the bottom surface of the thermoelectric element 15 may be a heat dissipation plate, and a top surface of the thermoelectric element 15 may be a heat absorption plate.

[0077] If a current is applied along the shared signal electrode 16, a current flows from the heat dissipation plate to the heat absorption plate and generates a temperature difference in both ends of the thermoelectric element 15. Also, the current is transferred from the thermoelectric element 15 to the ASIC 11 a, is transferred again to the piezoelectric layer 11, and vibrates the piezoelectric layer 11. The current that is transmitted to the piezoelectric layer 11 is discharged along the shared ground electrode 17 disposed on the piezoelectric layer 11.

[0078] Unlike in FIGS. 5A through 5C, FIGS. 5D and 5E illustrate various embodiments of the ultrasonic probe 110 in which the thermoelectric element 15 makes surface contact with the bottom surface of the piezoelectric layer 11 and the ASIC 11 a makes surface contact with the bottom surface of the thermoelectric element 15. Since the current controlled by the ASIC 11 a may be transferred to the piezoelectric layer 11 via the thermoelectric element 15, this embodiment may be implemented.

[0079] FIG. 5D illustrates the ultrasonic probe 110 including the shared ground electrode, in accordance with another embodiment of the present invention. The signal electrode 16a for the piezoelectric layer 11 may be disposed on the ASIC 11 a, and a current may be supplied via the signal electrode 16a for the piezoelectric layer 11. The supplied current may be transferred to the piezoelectric layer 11 via the thermoelectric element 15, and the piezoelectric layer 11 may vibrate due to the transferred current and may generate ultrasonic waves. The current that vibrates the piezoelectric layer 11 may be discharged through the shared ground electrode 17 disposed on the piezoelectric layer 11.

[0080] Also, the signal electrode 16b for the thermoelectric element 15 may be disposed on the bottom surface of the thermoelectric element 15. Thus, the bottom surface of the thermoelectric element 15 may be a heat dissipation plate that heats a contact surface between the piezoelectric layer 11 and the thermoelectric element 15, and the top surface of the thermoelectric element 15 may be a heat absorption plate that cools the contact surface between the piezoelectric layer 11 and the thermoelectric element 15. The current supplied through the signal electrode 16b for the thermoelectric element 15 may flow from the heat dissipation plate to the heat absorption plate and may generate a temperature difference in both ends of the thermoelectric element 15. The current that flows through the heat absorption plate may flow along the piezoelectric layer 11 and may be discharged along the shared ground electrode 17.

[0081] FIG. 5D is the same as FIG. 5B in that the number of ground electrodes is reduced to one and the weight or volume of the ultrasonic probe 110 may be reduced, unlike in FIG. 5A.

[0082] FIG. 5E illustrates the ultrasonic probe 110 including the shared ground electrode and the shared signal electrode, in accordance with still another embodiment of the present invention. The shared signal electrode 16 may be disposed on the ASIC 11 a, and a current that controls the thermoelectric element 15 and the piezoelectric layer 11 may be supplied through the shared signal electrode 16. Also, the shared ground electrode 17 may be disposed on the piezoelectric layer 11, and the supplied current may be discharged through the shared ground electrode 17.

[0083] Like in FIG. 5C, the number of electrodes is reduced to two, and there is no problem of the limitation in the internal space of the ultrasonic probe 110. Also, even

when the piezoelectric layer 11 and the thermoelectric element 15 are diced, the risk of generating an electrical short is low. In addition, interference that occurs between a plurality of electrode layers is reduced so that sound performance can be maintained.

[0084] The ultrasonic probe 110 illustrated in FIGS. 2A and 2B, FIG. 3, FIGS. 4A through 4C, and FIGS. 5A through 5E is a one-dimensional arrangement ultrasonic probe 110. However, even when the transducer device is arranged in a two-dimensional manner, the temperature of the piezoelectric layer 11 may be controlled through the thermoelectric element 15.

[0085] FIGS. 6A and 6B illustrate ultrasonic probes in which the piezoelectric layer 11 is diced, in accordance with other embodiments of the present invention. Arrows in FIGS. 6A and 6B mean a direction in which a current flows.

[0086] Even when the piezoelectric layer 11 is diced into a plurality of channels, temperature of the piezoelectric layer 11 may be controlled using the thermoelectric element 15. In detail, the piezoelectric layer 11 may be diced into and may include one or more piezoelectric channels. In this case, the piezoelectric layer 11 needs to be maintained at an appropriate temperature at which each piezoelectric channel operates normally. To this end, the thermoelectric element 15 including one or more thermoelectric channels may contact the piezoelectric layer 11. In particular, the thermoelectric element 15 may be diced into one or more thermoelectric channels, and each piezoelectric channel may contact each thermoelectric channel. Thus, temperature of each piezoelectric channel may be controlled by each thermoelectric channel.

[0087] FIG. 6A illustrates the ultrasonic probe 110 in which the thermoelectric element 15 makes surface contact with the piezoelectric layer 11 diced into one or more channels, in accordance with an embodiment of the present invention. Like in FIG. 6A, since the piezoelectric layer 11 includes one or more piezoelectric channels, the thermoelectric element 15 needs to be provided to contact each piezoelectric channel. To this end, the thermoelectric element 15 is diced into one or more thermoelectric channels and is provided to make surface contact with the piezoelectric layer 11.

[0088] FIG. 6B illustrates the ultrasonic probe 110 in which the ASIC 11 a makes surface contact with the piezoelectric layer 11 diced into one or more channels and the diced thermoelectric element 15 makes surface contact with the ASIC 11 a, in accordance with another embodiment of the present invention. Even when the ASIC 11 a makes surface contact with the piezoelectric layer 11, the thermoelectric element 15 diced in the same manner as FIG. 6A may control temperature of the piezoelectric layer 11. If each thermoelectric channel makes surface contact with the ASIC 11 a so as to maintain temperature of each piezoelectric channel that makes surface contact with the ASIC 11 a, heat exchange between the piezoelectric channel and the thermoelectric

channel may be performed by the ASIC 11 a.

[0089] When the piezoelectric layer 11 is diced into one or more piezoelectric channels, the thermoelectric element 15 may be a thin film type thermoelectric element 15 so that the thermoelectric element 15 can be diced into one or more thermoelectric channels.

[0090] FIG. 7 is a control block diagram of an ultrasonic imaging apparatus including an ultrasonic probe in which a thermoelectric element is disposed, in accordance with an embodiment of the present invention.

[0091] The ultrasonic probe 110 may include the piezoelectric layer 11 that vibrates and generates ultrasonic waves, the thermoelectric element 15 that controls temperature of the piezoelectric layer 11, and a temperature sensor 20 that senses the temperature of the piezoelectric layer 11.

[0092] When the temperature of the piezoelectric layer 11 rises due to its vibration or decreases in an extremely low temperature environment, the piezoelectric layer may not operate normally. Thus, the temperature of the piezoelectric layer 11 needs to be maintained at an appropriate level.

[0093] To this end, the thermoelectric element 15 may contact one surface of the piezoelectric layer 11 or may make surface contact with the piezoelectric layer 11 and may contract one surface of the ASIC 11 a that transfers a current. If a current is supplied to the thermoelectric element 15, a temperature difference is generated in both ends of the thermoelectric element 15, and thus, temperature of the piezoelectric layer 11 may be controlled using the temperature difference.

[0094] In detail, the thermoelectric element 15 may include a heat dissipation plate that dissipates heat toward a contact surface between the piezoelectric layer 11 and the thermoelectric element 15 and heats the contact surface, and a heat absorption plate that absorbs heat of the contact surface and cools the contact surface. The heat dissipation plate or the heat absorption plate contacts the piezoelectric layer 11 in consideration of an environment in which ultrasonic diagnosis is performed, so that the piezoelectric layer 11 may be heated or cooled.

[0095] The temperature sensor 20 may be disposed at an inner side of a housing and may sense the temperature of the piezoelectric layer 11. To this end, the temperature sensor 20 may be disposed to contact the piezoelectric layer 11. If it is determined that the temperature sensor 20 senses the temperature of the piezoelectric layer 11 and determines that the piezoelectric layer 11 is at a predetermined temperature or more or less, the result of determination may be transmitted to a controller 170 provided on the body 100.

[0096] The controller 170 may receive the result of sensing temperature from the temperature sensor 20 and may control a supply current supplied to the thermoelectric element 15 based on the result of sensing temperature. Since it is determined that temperature of the piezoelectric layer 11 is at an appropriate level or more or less, the controller 170 may control the ultrasonic imaging

apparatus to supply a current to the thermoelectric element 15 and to cool or heat the piezoelectric layer 11. The controller 170 may include a processor and may be implemented with hardware.

[0097] In the ultrasonic probe 110 and the ultrasonic imaging apparatus including the same according to the one or more embodiments of the present invention, the piezoelectric layer 11 disposed in the ultrasonic probe 110 and the thermoelectric element 15 may make surface contact with each other directly or through the ASIC 11 a so that the temperature of the piezoelectric layer 11 can be maintained in an optimum state. Accordingly, smooth ultrasonic diagnosis can be performed, and a patient's safety can be maintained.

[0098] As described above, in an ultrasonic probe and an ultrasonic imaging apparatus having the same according to the one or more embodiments of the present invention, a piezoelectric layer is heated or cooled using a thermoelectric element so that an inner side of the ultrasonic probe can be always maintained at an appropriate temperature.

[0099] In addition, an internal structure of the ultrasonic probe can be simplified by integrating electrodes of the thermoelectric element with electrodes of the piezoelectric layer.

[0100] Although a few embodiments of the present invention have been shown and described, it would be appreciated by those skilled in the art that changes may be made in these embodiments without departing from the principles and spirit of the invention, the scope of which is defined in the claims and their equivalents.

Claims

1. An ultrasonic probe comprising:

a piezoelectric layer that vibrates and generates ultrasonic waves if a current is supplied to the piezoelectric layer; and
a thermoelectric element that contacts one surface of the piezoelectric layer and controls temperature of the piezoelectric layer if a current is supplied to the thermoelectric element.

2. The ultrasonic probe of claim 1, wherein the thermoelectric element comprises:

a heat dissipation plate that is disposed on one surface of the thermoelectric element and dissipates heat toward a contact surface between the piezoelectric layer and the thermoelectric element; and
a heat absorption plate that is disposed at an opposite side to the heat dissipation plate and absorbs heat of the contact surface.

3. The ultrasonic probe of claim 2, wherein the thermo-

electric element contacts the piezoelectric layer through the heat dissipation plate and heats the piezoelectric layer.

5 **4.** The ultrasonic probe of claim 2, wherein the thermoelectric element contacts the piezoelectric layer through the heat absorption plate and cools the piezoelectric layer.

10 **5.** The ultrasonic probe of claim 1, wherein the piezoelectric layer and the thermoelectric element share a signal electrode through which a current is supplied to the piezoelectric layer and the thermoelectric element, respectively.

15 **6.** The ultrasonic probe of claim 1, wherein the piezoelectric layer and the thermoelectric element share a ground electrode.

20 **7.** The ultrasonic probe of claim 1, wherein, when the piezoelectric layer comprises one or more piezoelectric channels, the thermoelectric element comprises one or more thermoelectric channels corresponding to the one or more piezoelectric channels.

25 **8.** An ultrasonic probe comprising:

a piezoelectric layer that vibrates and generates ultrasonic waves if a current is supplied to the piezoelectric layer;
an application specific integrated circuit (ASIC) that transfers the current to the piezoelectric layer; and
a thermoelectric element that contacts one surface of the ASIC and controls temperature of the piezoelectric layer if a current is supplied to the thermoelectric element.

35 **9.** The ultrasonic probe of claim 8, wherein the thermoelectric element comprises:

a heat dissipation plate that is disposed on one surface of the thermoelectric element and dissipates heat toward a contact surface between the piezoelectric layer and the thermoelectric element; and
a heat absorption plate that is disposed at an opposite side to the heat dissipation plate and absorbs heat of the contact surface.

40 **10.** The ultrasonic probe of claim 8, wherein the piezoelectric layer and the thermoelectric element share a signal electrode through which a current is supplied to the piezoelectric layer and the thermoelectric element, respectively.

45 **11.** The ultrasonic probe of claim 8, wherein the piezoelectric layer and the thermoelectric element share

a ground electrode.

12. An ultrasonic imaging apparatus comprising:

an ultrasonic probe comprising a piezoelectric layer that vibrates and generates ultrasonic waves, a thermoelectric element that contacts one surface of the piezoelectric layer and controls temperature of the piezoelectric layer according to a supplied current, and a temperature sensor that senses the temperature of the piezoelectric layer; and
 a controller that controls the supplied current based on the sensed temperature.

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13. An ultrasonic imaging apparatus comprising:

an ultrasonic probe comprising a piezoelectric layer that vibrates and generates ultrasonic waves, an application specific integrated circuit (ASIC) that transfers a current to the piezoelectric layer, a thermoelectric element that contacts one surface of the ASIC and controls temperature of the piezoelectric layer according to the supplied current, and a temperature sensor that senses the temperature of the piezoelectric layer; and
 a controller that controls the supplied current based on the sensed temperature.

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FIG. 1

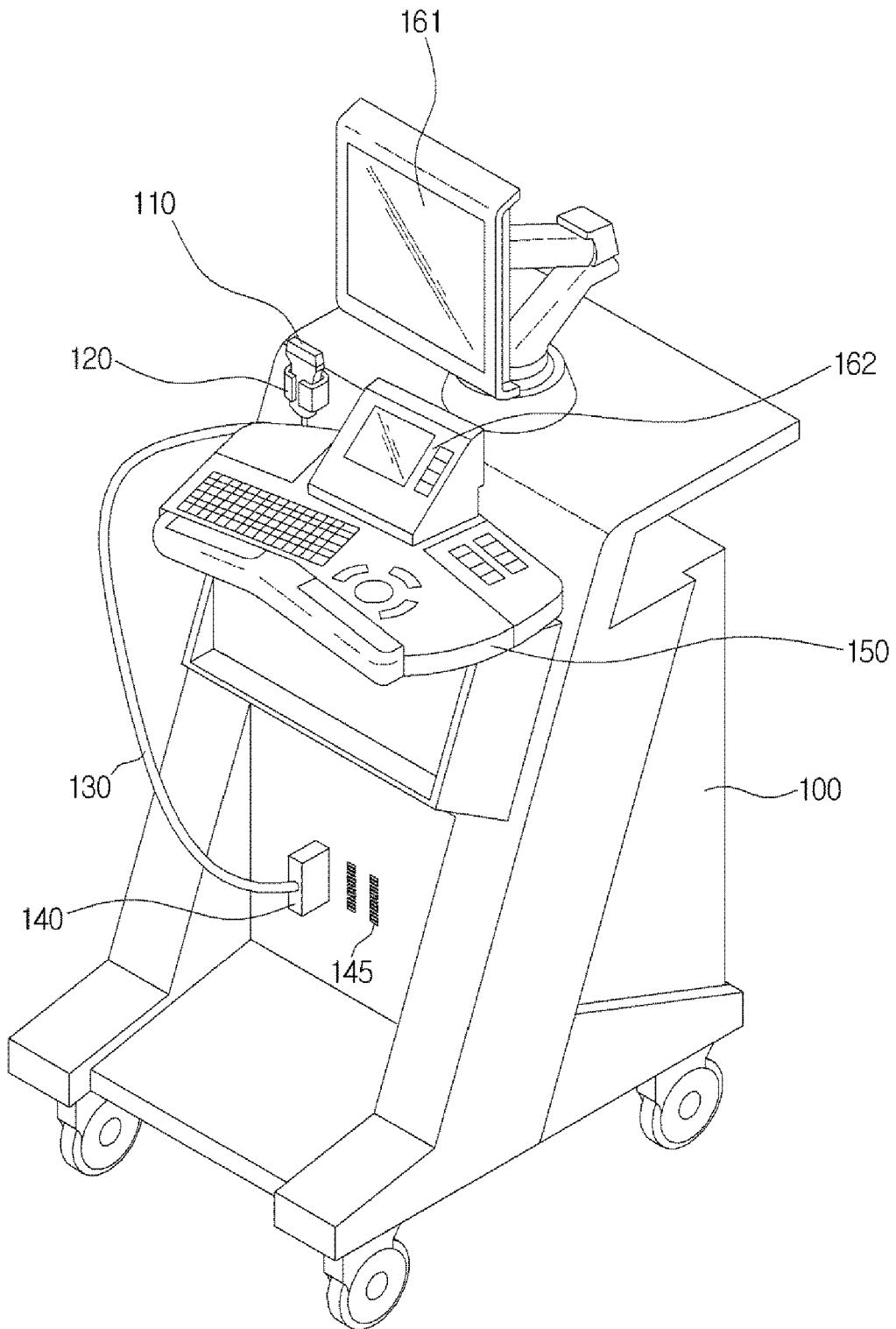


FIG. 2A

110

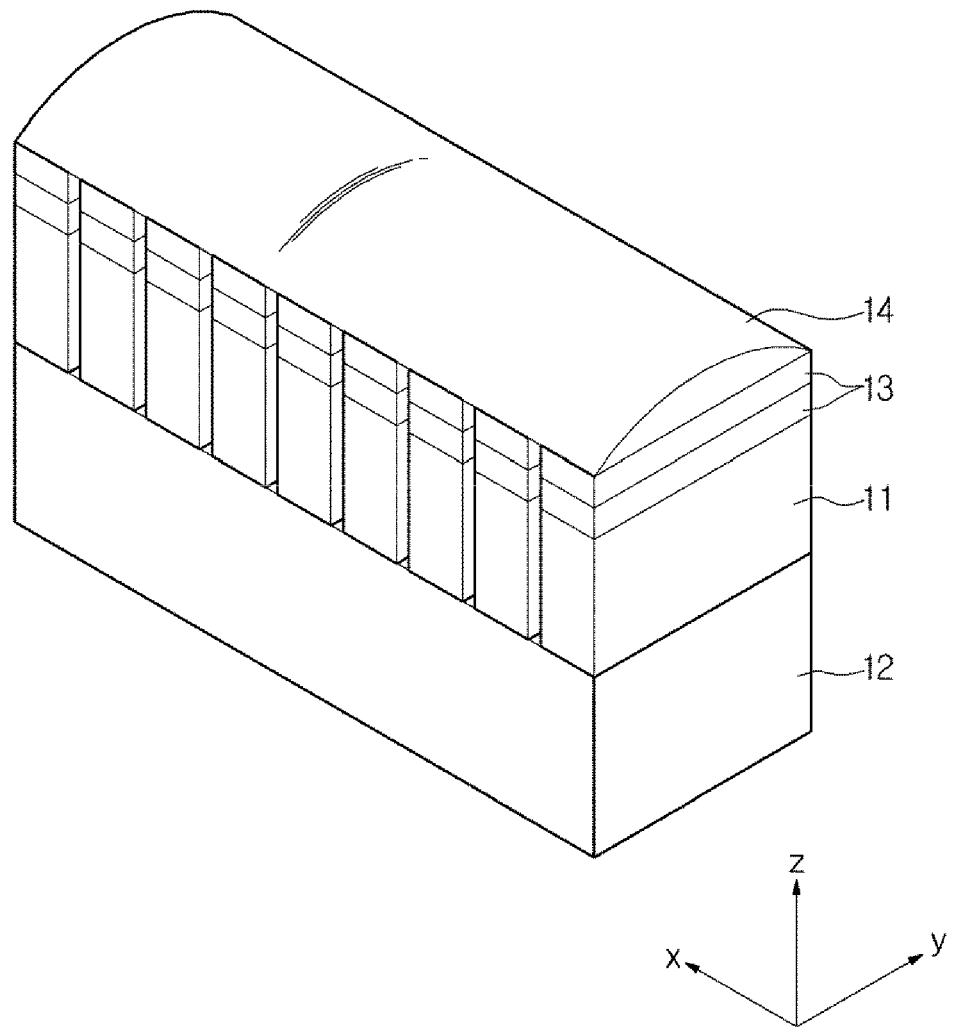


FIG. 2B

110

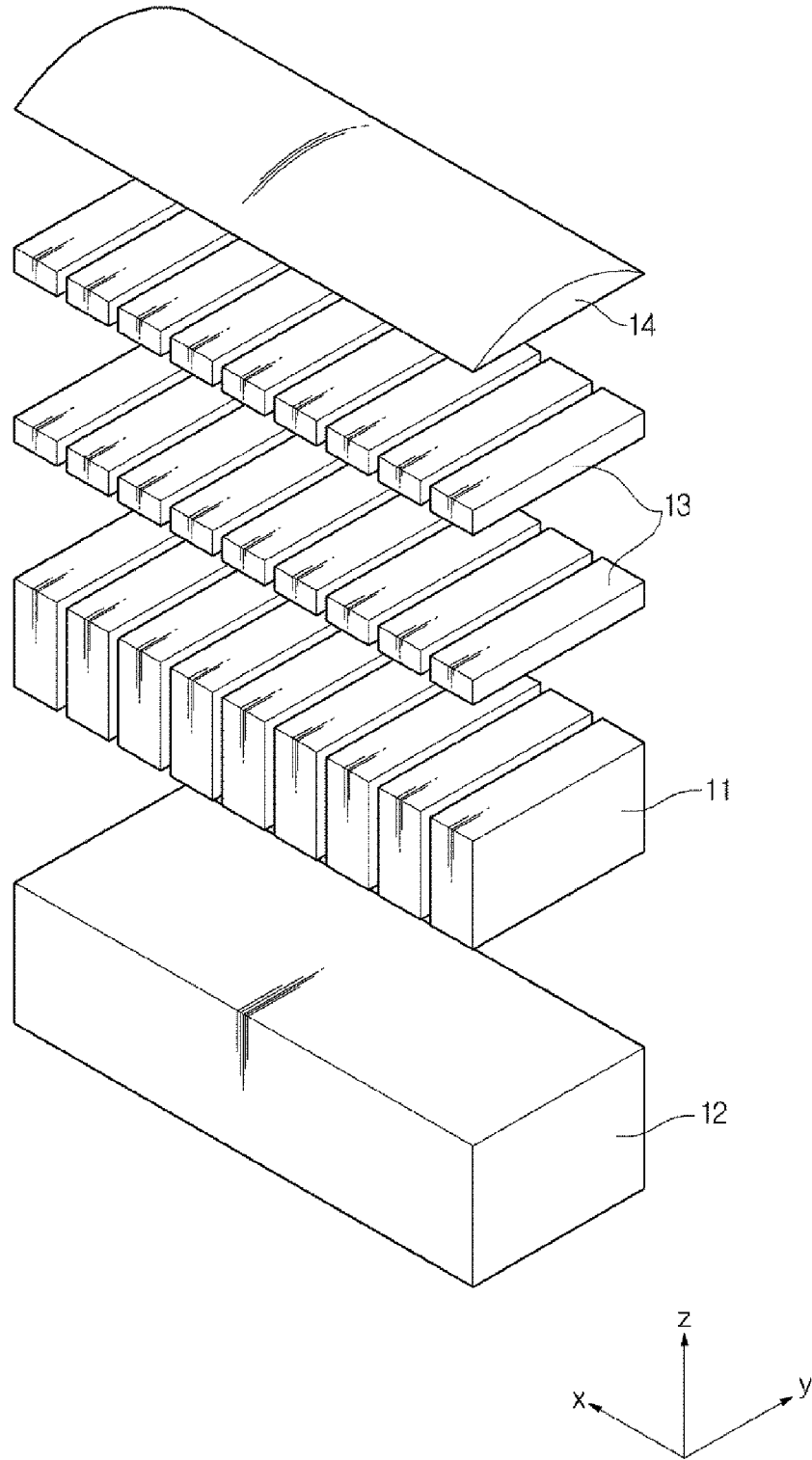


FIG. 3

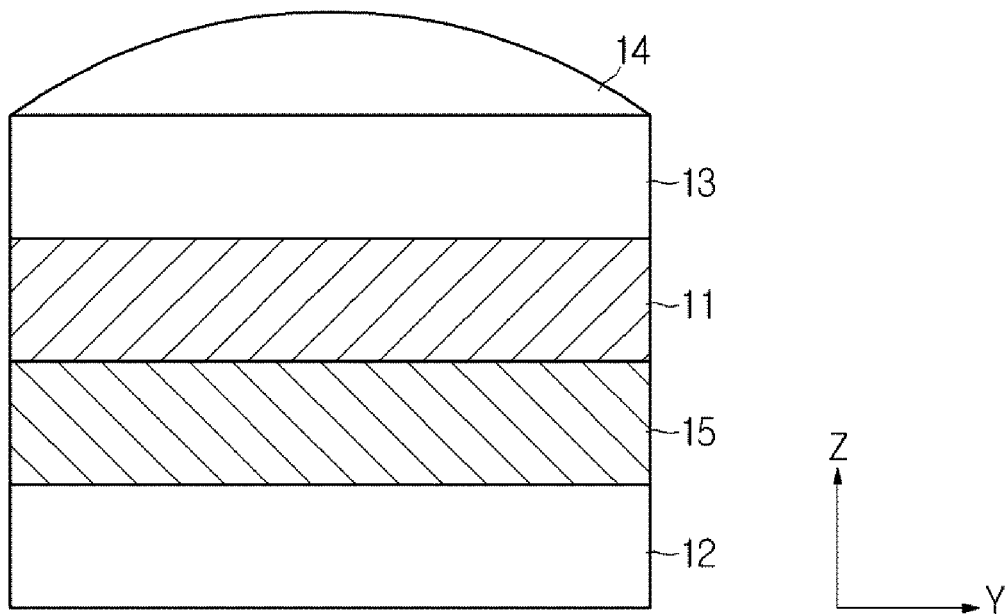


FIG. 4A

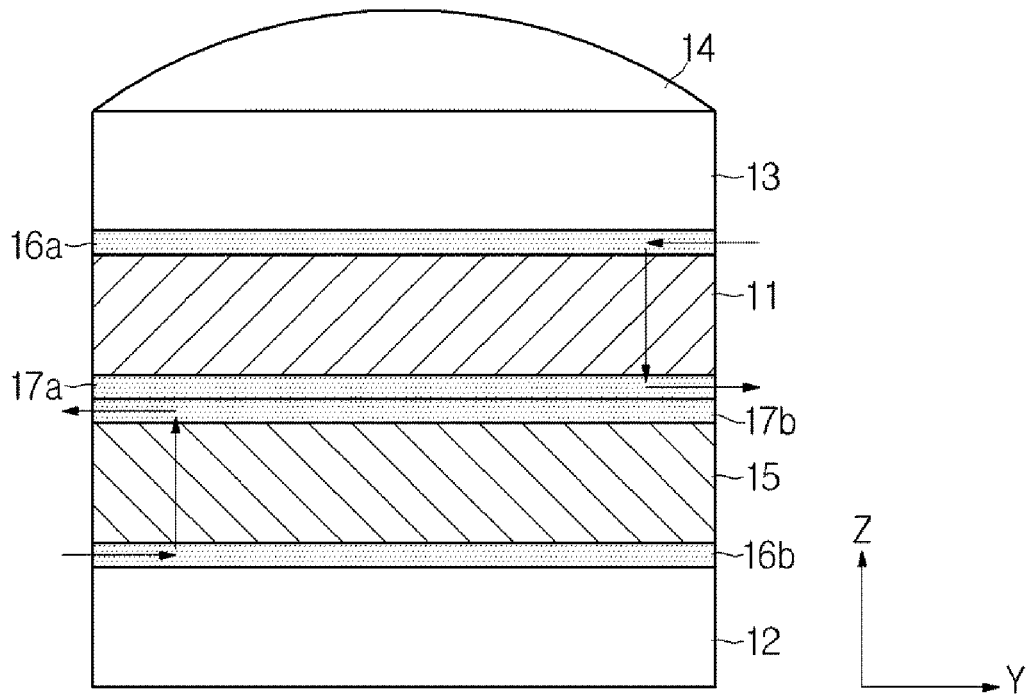


FIG. 4B

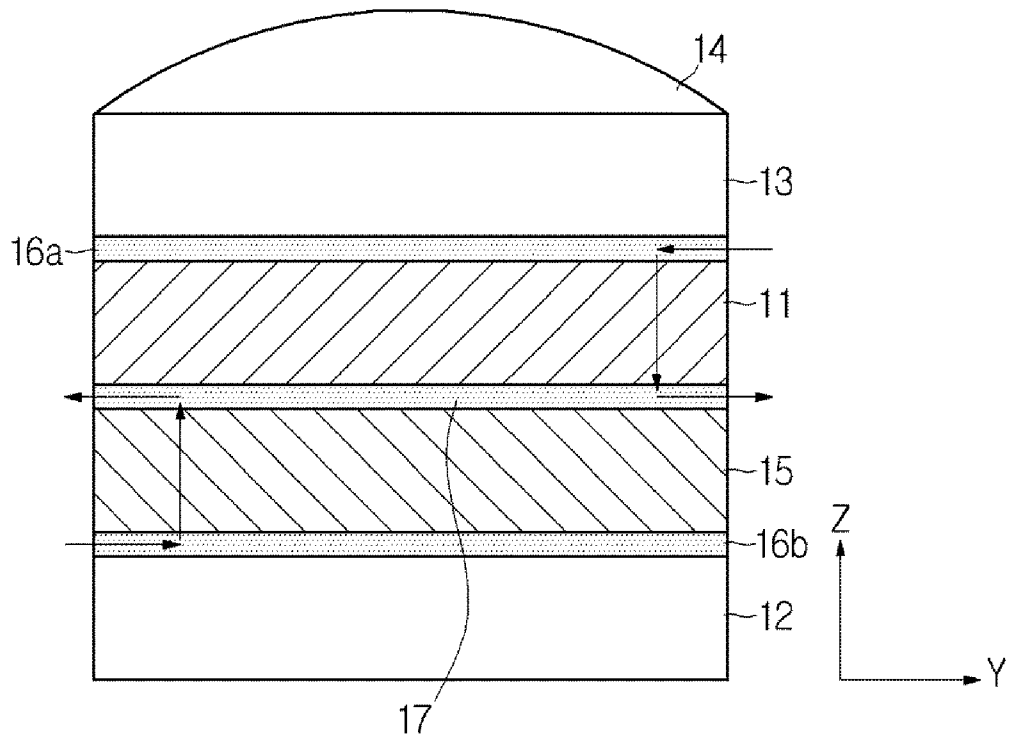


FIG. 4C

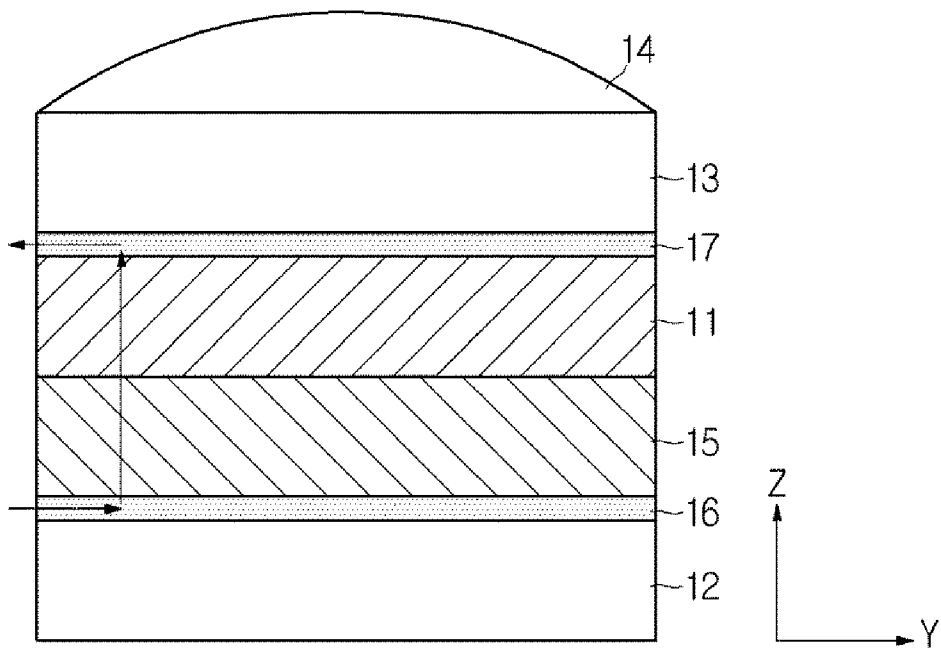


FIG. 5A

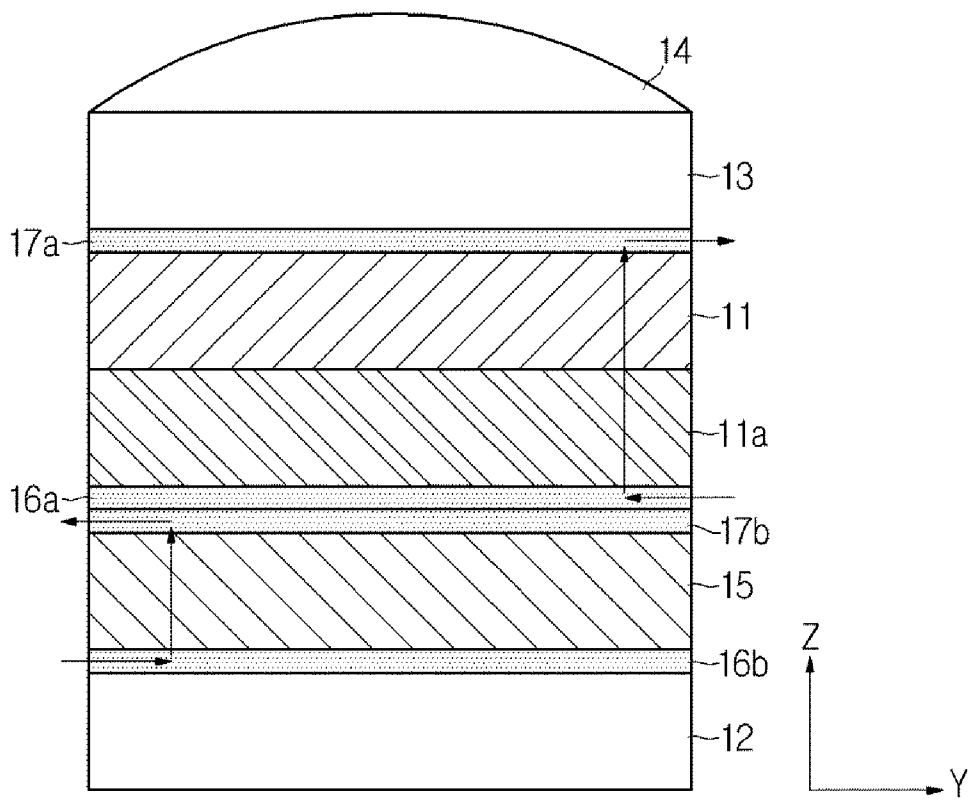


FIG. 5B

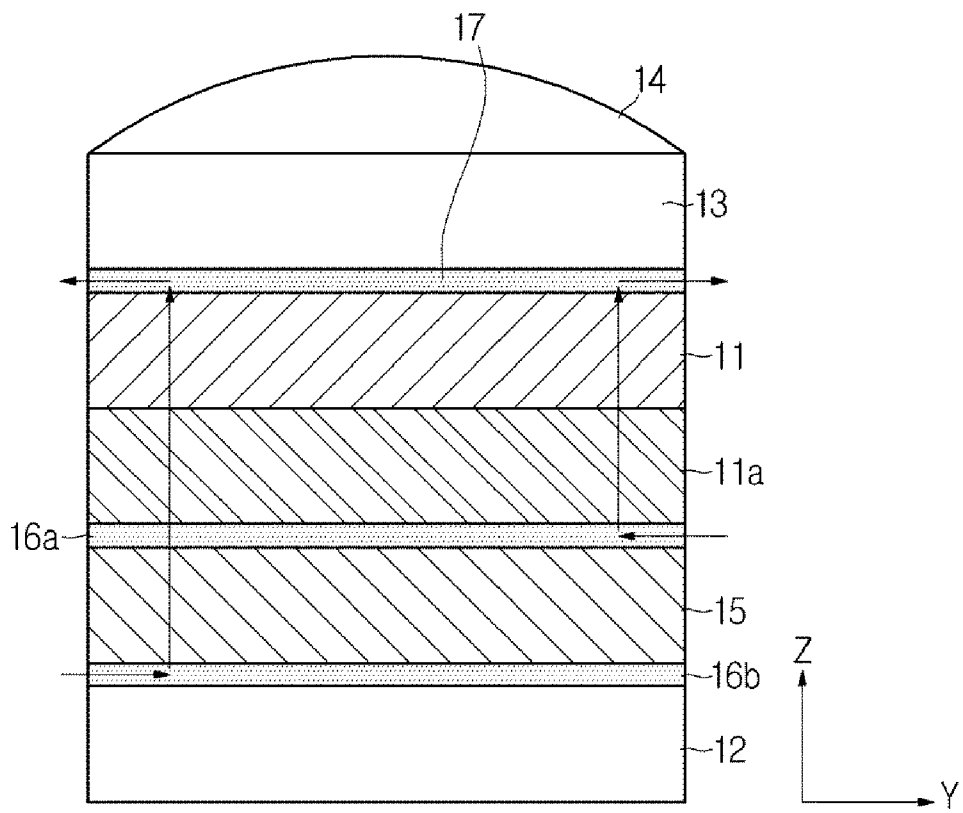


FIG. 5C

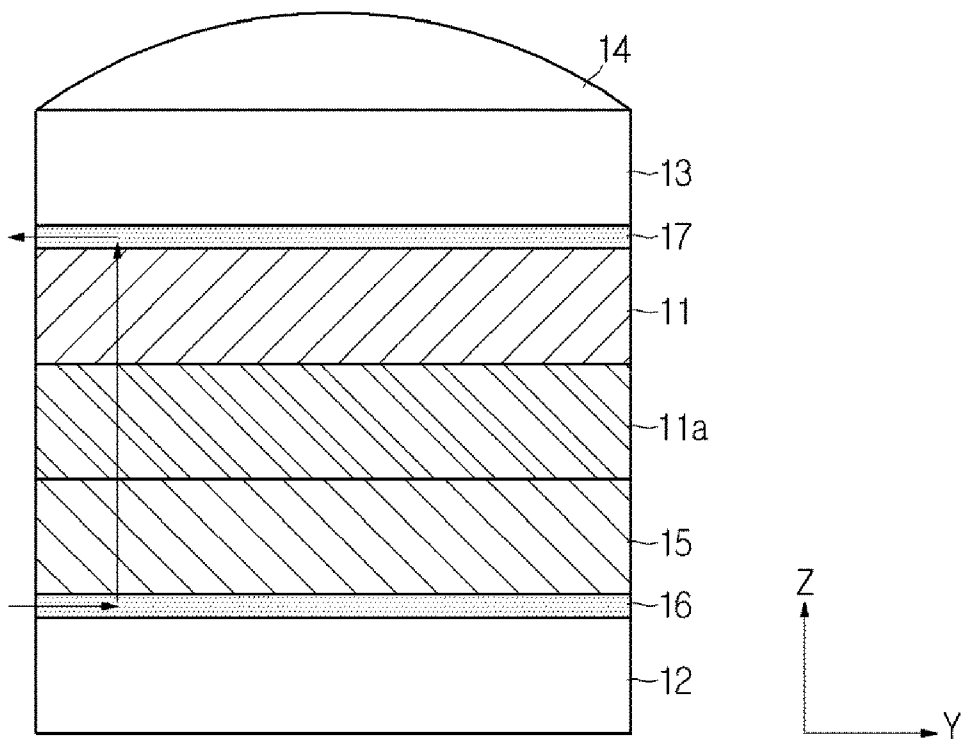


FIG. 5D

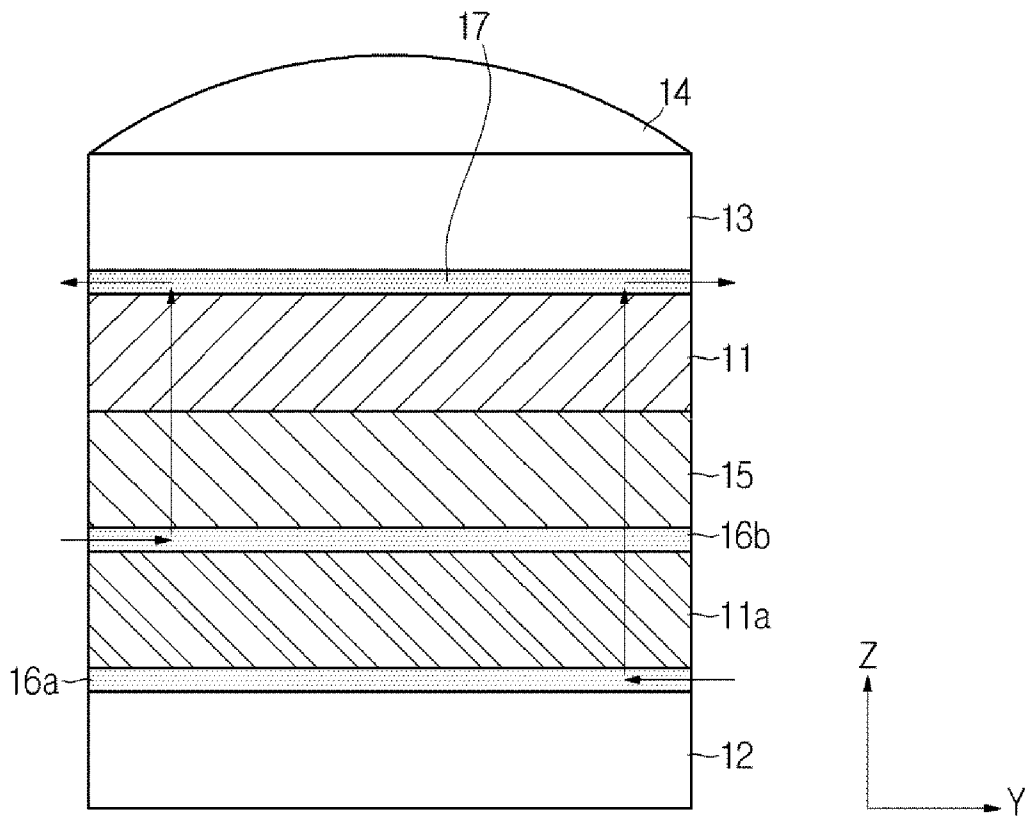


FIG. 5E

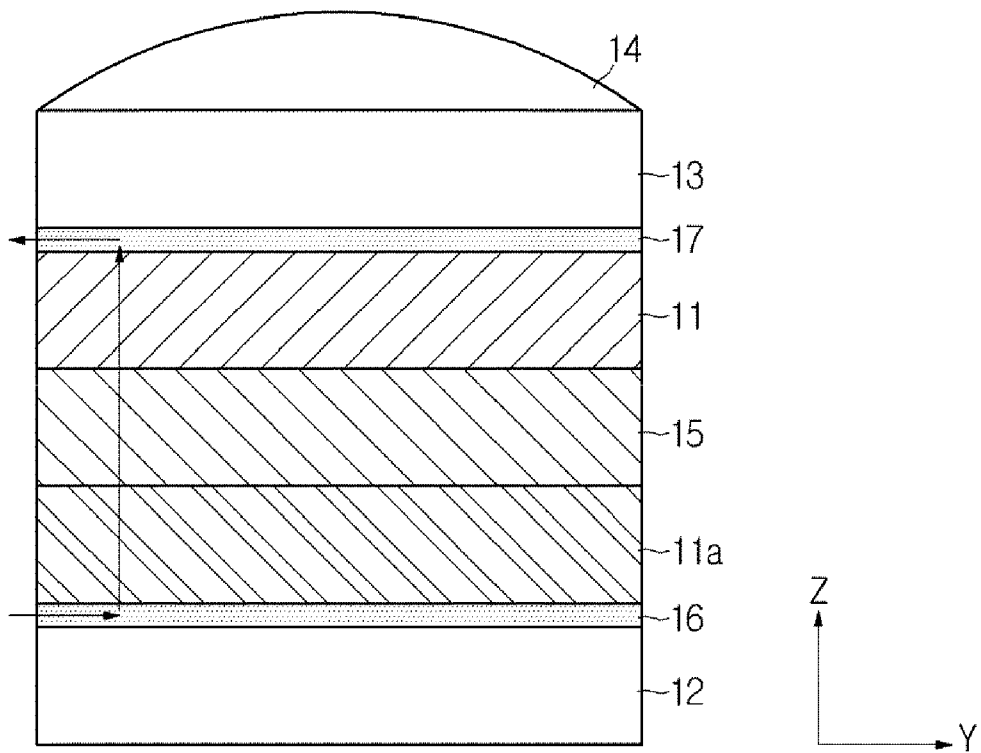


FIG. 6B

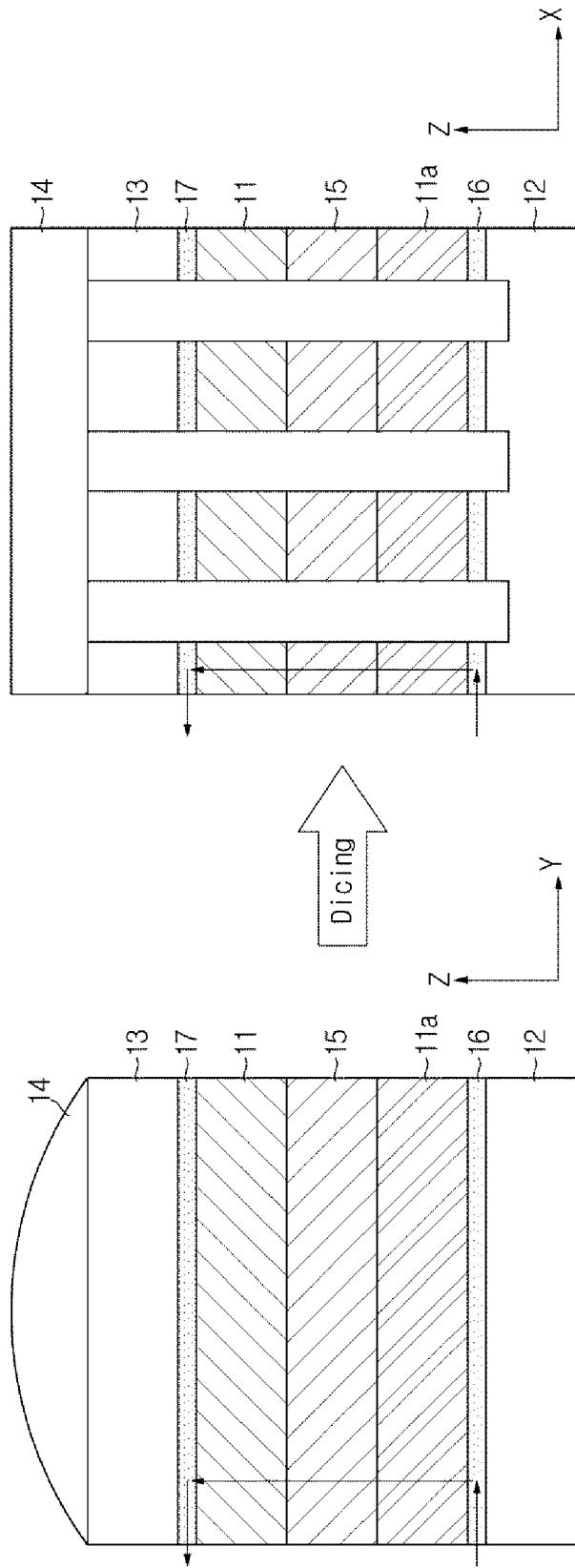
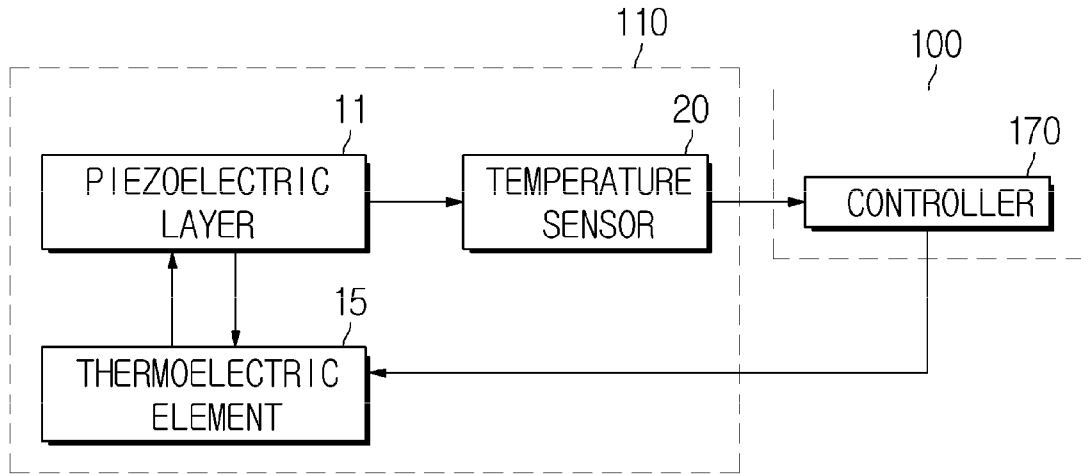


FIG. 7





EUROPEAN SEARCH REPORT

Application Number
EP 14 18 2591

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DOCUMENTS CONSIDERED TO BE RELEVANT			
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (IPC)
X	WO 2013/140298 A2 (KONINKL PHILIPS NV [NL]) 26 September 2013 (2013-09-26) * abstract * * figures 1,2 * * page 6, line 2 - page 6, line 10 * * page 11, line 16 - page 11, line 31 *	1-13	INV. A61B8/00 B06B1/06 H01L41/08
X	US 2008/139974 A1 (DA SILVA LUIZ B [US]) 12 June 2008 (2008-06-12) * abstract * * figure 5 * * paragraph [0057] - paragraph [0059] *	1	
A	JP 2013 146478 A (KONICA MINOLTA INC) 1 August 2013 (2013-08-01) * abstract; figures 1-9 * * paragraph [0024] *	5,6,10,11	
A	US 2009/287086 A1 (HYUGA HIROAKI [JP]) 19 November 2009 (2009-11-19) * abstract * * figure 1 * * paragraph [0033] - paragraph [0040] *	1-13	
			TECHNICAL FIELDS SEARCHED (IPC)
			A61B B06B H01L
The present search report has been drawn up for all claims			
Place of search Munich		Date of completion of the search 24 April 2015	Examiner Moehrs, Sascha
CATEGORY OF CITED DOCUMENTS X : particularly relevant if taken alone Y : particularly relevant if combined with another document of the same category A : technological background O : non-written disclosure P : intermediate document		T : theory or principle underlying the invention E : earlier patent document, but published on, or after the filing date D : document cited in the application L : document cited for other reasons & : member of the same patent family, corresponding document	

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ANNEX TO THE EUROPEAN SEARCH REPORT
ON EUROPEAN PATENT APPLICATION NO.

EP 14 18 2591

5

This annex lists the patent family members relating to the patent documents cited in the above-mentioned European search report. The members are as contained in the European Patent Office EDP file on
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24-04-2015

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Patent document cited in search report	Publication date	Patent family member(s)	Publication date
WO 2013140298 A2	26-09-2013	CN 104205207 A	10-12-2014
		EP 2828846 A2	28-01-2015
		US 2015045670 A1	12-02-2015
		WO 2013140298 A2	26-09-2013

US 2008139974 A1	12-06-2008	CN 101622031 A	06-01-2010
		EP 2101876 A2	23-09-2009
		TW 200831152 A	01-08-2008
		US 2008139974 A1	12-06-2008
WO 2008070580 A2	12-06-2008		

JP 2013146478 A	01-08-2013	NONE	

US 2009287086 A1	19-11-2009	EP 2145697 A2	20-01-2010
		JP 2009273838 A	26-11-2009
		US 2009287086 A1	19-11-2009

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For more details about this annex : see Official Journal of the European Patent Office, No. 12/82

专利名称(译)	超声探头和具有该超声探头的超声成像设备		
公开(公告)号	EP2878269A1	公开(公告)日	2015-06-03
申请号	EP2014182591	申请日	2014-08-28
[标]申请(专利权)人(译)	三星麦迪森株式会社		
申请(专利权)人(译)	三星MEDISON CO. , LTD.		
当前申请(专利权)人(译)	三星MEDISON CO. , LTD.		
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IPC分类号	A61B8/00 B06B1/06 H01L41/08		
CPC分类号	A61B8/4209 A61B8/4405 A61B8/4444 A61B8/4483 A61B8/546 B06B1/0622 A61B8/5207 A61B8/5223		
优先权	1020130129098 2013-10-29 KR		
外部链接	Espacenet		

摘要(译)

本发明提供一种使用热电元件控制压电层温度的超声波探头和具有该超声波探头的超声波成像装置。超声波探头包括：压电层，如果向压电层提供电流，则振动并产生超声波；和热电元件，其接触压电层的一个表面，并且如果向热电元件提供电流则控制压电层的温度。

