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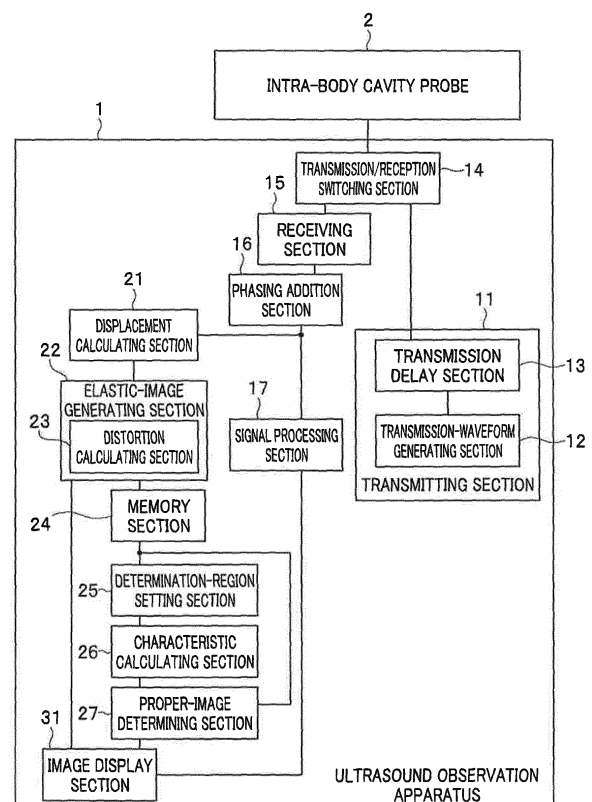
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(54) **ULTRASOUND OBSERVATION APPARATUS, ULTRASOUND OBSERVATION SYSTEM, AND METHOD FOR OPERATING ULTRASOUND OBSERVATION APPARATUS**

(57) An ultrasound observation apparatus (1) including a displacement calculating section (21) that measures displacement of a subject based on an ultrasound signal, an elastic-image generating section (22) that generates an elastic image based on the measured displacement, a memory section (24) that stores generated one or more elastic images, a determination-region setting section (25) that sets a proper-image determination region for proper image determination in the elastic image according to a size of an ROI, a characteristic calculating section (26) that calculates a region characteristic of the proper-image determination region, and a proper-image determining section (27) that determines based on the region characteristic whether the elastic image is a proper image.

FIG. 1



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Description

Technical Field

[0001] The present invention relates to an ultrasound observation apparatus, an ultrasound observation system, and an actuation method for the ultrasound observation apparatus for generating an image including an elastic image based on an ultrasound signal obtained by transmitting and receiving ultrasound.

Background Art

[0002] An ultrasound observation apparatus that generates, from a distortion amount of a biological tissue caused by an oppression force, an elastic image representing hardness or softness of the biological tissue has been put to practical use.

[0003] A series of images acquired in such an ultrasound observation apparatus are once stored in an image memory or the like. A user selects, out of the series of images stored in the image memory, a proper image as an image for calculating elasticity information and an image for medical record storage.

[0004] Incidentally, when the ultrasound observation apparatus is set in an elastic image observation mode, a region having a distortion amount is larger than a predetermined threshold in an image is sometimes colored and displayed. However, not all frame images are always colored. Therefore, when the user selects the proper image, the user needs to search for the proper image not only in colored frame images but also uncolored frame images. It takes a lot of time and labor for the selection of the proper image.

[0005] In order to cope with such a point, for example, International Publication No. 2011/010626 discloses a technique for automatically extracting a proper image based on an oppression state to an organism. References used for extraction in the publication are an average of displacement, an average of elasticity information, displacement of pressure, fluctuation in pressure in a beam line direction, and the like.

[0006] Japanese Patent Application Laid-Open Publication No. 2012-213545 discloses an ultrasound diagnostic apparatus that, in order to provide a high-quality three-dimensional elastic image, determines elastic volume data formed by a plurality of two-dimensional elastic image including a noise image as a noise volume and hides a three-dimensional elastic image by the elastic volume data determined as the noise volume.

[0007] Further, Japanese Patent Application Laid-Open Publication No. 2005-118152 describes a technique for, in order to provide a high-quality elastic image, evaluating, based on various data (pressure data, displacement frame data, and elastic frame data) used in a generation process of a distortion elastic image (elastic frame data), a value of performing image display concerning respective measurement points in a region of

interest (ROI), distinguishing useless information and useful information, and finally not leaving (masking to hide) the useless information as an image.

[0008] However, in an ultrasound diagnostic apparatus described in International Publication No. 2011/010626, the proper image cannot be drawn because of, for example, reasons (1) and (2) below.

(1) In the case of a small probe like an intra-body cavity probe of an ultrasound endoscope or the like, since a curvature radius of the probe is small, if an ROI (region of interest) size for elastic image display is large, pressures in all beam line directions are not uniformly applied.

(2) In the case of the intra-body cavity probe of the ultrasound endoscope or the like, it is difficult to cause displacement with oppression of a surgeon. Displacement by a beat or a pulsation is used as displacement of an organism. Therefore, stable pressure is obtained only in a direction in which a displacement source such as the beat or the pulsation is present.

[0009] The techniques described in Japanese Patent Application Laid-Open Publication No. 2012-213545 and Japanese Patent Application Laid-Open Publication No. 2005-118152 do not take into account the same problems.

[0010] The present invention has been devised in view of the circumstances and it is an object of the present invention to provide an ultrasound observation apparatus, an ultrasound observation system, and an actuation method for the ultrasound observation apparatus that can automatically extract a proper image without depending on an ROI size.

Disclosure of Invention

Means for Solving the Problem

[0011] An ultrasound observation apparatus according to an aspect of the present invention is an ultrasound observation apparatus that generates an ultrasound image based on an ultrasound signal generated from ultrasound transmitted to a subject and reflected, the ultrasound observation apparatus including: a transmitting section that transmits a driving signal for generating the ultrasound transmitted to the subject; a receiving section that receives the ultrasound signal generated from the ultrasound reflected by the subject; a displacement calculating section that measures displacement of the subject based on the ultrasound signal received by the receiving section; an elastic-image generating section that generates an elastic image based on the displacement measured by the displacement calculating section; a storing section that stores one or more of the elastic images generated by the elastic-image generating section; a determination-region setting section that sets, accord-

ing to a size of an ROI, which is a region of interest, a proper-image determination region for determining a proper image out of the one or more elastic images stored in the storing section; a characteristic calculating section that calculates a region characteristic of the proper-image determination region; and a proper-image determining section that determines based on the region characteristic whether the elastic image in which the proper-image determination region is set is the proper image.

[0012] An ultrasound observation system according to an aspect of the present invention includes: the ultrasound observation apparatus; and an ultrasound probe that receives the driving signal transmitted from the transmitting section, transmits the ultrasound to the subject, receives the ultrasound reflected by the subject, generates the ultrasound signal, and transmits the ultrasound signal to the receiving section.

[0013] An actuation method for an ultrasound observation apparatus according to an aspect of the present invention is an actuation method for an ultrasound observation apparatus that generates an ultrasound image based on an ultrasound signal generated from ultrasound transmitted to a subject and reflected, the actuation method for the ultrasound observation apparatus including: a step in which a transmitting section transmits a driving signal for generating the ultrasound transmitted to the subject; a step in which a receiving section receives the ultrasound signal generated from the ultrasound reflected by the subject; a step in which a displacement calculating section measures displacement of the subject based on the ultrasound signal received by the receiving section; a step in which an elastic-image generating section generates an elastic image based on the displacement measured by the displacement calculating section; a step in which a storing section stores one or more of the elastic images generated by the elastic-image generating section; a step in which a determination-region setting section sets, according to a size of an ROI, which is a region of interest, a proper-image determination region for determining a proper image out of the one or more elastic images stored in the storing section; a step in which a characteristic calculating section calculates a region characteristic of the proper-image determination region; and a step in which a proper-image determining section determines based on the region characteristic whether the elastic image in which the proper-image determination region is set is the proper image.

Brief Description of the Drawings

[0014]

Fig. 1 is a block diagram showing a configuration of an ultrasound observation system in a first embodiment of the present invention;

Fig. 2 is a diagram showing a state in which a region where a distortion amount in an ROI is equal to or larger than a predetermined value is displayed in the

first embodiment;

Fig. 3 is a diagram showing an example of a position of a displacement source with respect to the ROI in the first embodiment;

Fig. 4 is a diagram showing an example of a proper-image determination region set when a center angle of the ROI is larger than a predetermined threshold in the first embodiment;

Fig. 5 is a diagram showing an example of a proper-image determination region set when the center angle of the ROI is equal to or smaller than the predetermined threshold;

Fig. 6 is a diagram showing an example of a first position in sequentially scanning the proper-image determination region in the ROI of the first embodiment;

Fig. 7 is a diagram showing an example of a second position in sequentially scanning the proper-image determination region in the ROI of the first embodiment;

Fig. 8 is a diagram showing an example of a third position in sequentially scanning the proper-image determination region in the ROI of the first embodiment;

Fig. 9 is a diagram showing an example in which the proper-image determination region is divided by a fixed value in the ROI of the first embodiment;

Fig. 10 is a diagram showing a first division example in dividing the proper-image determination region by a variable value in the ROI of the first embodiment;

Fig. 11 is a diagram showing a second division example in dividing the proper-image determination region by a variable value in the ROI of the first embodiment;

Fig. 12 is a diagram showing a third division example in dividing the proper-image determination region by a variable value in the ROI of the first embodiment;

Fig. 13 is a flowchart showing elastic-image extraction processing in an ultrasound observation system of the first embodiment;

Fig. 14 is a flowchart showing single region processing in the first embodiment;

Fig. 15 is a flowchart showing sequential scan processing in the first embodiment;

Fig. 16 is a flowchart showing fixed-value division processing in the first embodiment; and

Fig. 17 is a flowchart showing variable-value division processing in the first embodiment.

50 Best Mode for Carrying Out the Invention

[0015] An embodiment of the present invention is explained below with reference to the drawings.

55 [First embodiment]

[0016] Fig. 1 to Fig. 17 show a first embodiment of the present invention. Fig. 1 is a block diagram showing a

configuration of an ultrasound observation system.

[0017] The ultrasound observation system includes an intra-body cavity probe 2 that transmits ultrasound to a subject and receives the ultrasound reflected by the subject and an ultrasound observation apparatus 1 that generates an ultrasound image based on an ultrasound signal obtained from the received ultrasound.

[0018] The intra-body cavity probe 2 is an ultrasound probe inserted into a body cavity and used. The intra-body cavity probe 2 includes an ultrasound transducer configured by arraying a large number of vibration elements, transmits ultrasound from an ultrasound transmission/reception surface of the ultrasound transducer to the subject, receives, on the ultrasound transmission/reception surface of the ultrasound transducer, the ultrasound reflected by the subject, and generates an ultrasound signal from the received ultrasound. Specifically, the intra-body cavity probe 2 is configured as an ultrasound probe of a convex type, an ultrasound probe of a radial type, or the like.

[0019] The ultrasound observation apparatus 1 includes a transmitting section 11, a transmission/reception switching section 14, a receiving section 15, a phasing addition section 16, a signal processing section 17, a displacement calculating section 21, an elastic-image generating section 22, a memory section 24, a determination-region setting section 25, a characteristic calculating section 26, a proper-image determining section 27, and an image display section 31.

[0020] The transmitting section 11 transmits a driving signal for generating ultrasound transmitted to a subject. The transmitting section 11 includes a transmission-waveform generating section 12 and a transmission delay section 13.

[0021] The transmission-waveform generating section 12 generates a signal waveform for driving the respective vibration elements configuring the ultrasound transducer and outputs the signal waveform as a driving signal.

[0022] The transmission delay section 13 delays the driving signal generated by the transmission-waveform generating section 12 to thereby adjust driving timing of the respective vibration elements configuring the ultrasound transducer. Consequently, a focus and a direction of an ultrasound beam transmitted from the ultrasound transducer are controlled. The ultrasound can be converged in a desired position (depth).

[0023] The transmission/reception switching section 14 includes, for example, a multiplexer that sequentially selects a plurality of vibration elements for performing transmission and reception of the ultrasound. The transmission/reception switching section 14 transmits the driving signal, which is transmitted from the transmitting section 11, to the ultrasound transducer and transmits an ultrasound signal (an echo signal), which is transmitted from the ultrasound transducer, to the receiving section 15.

[0024] The receiving section 15 receives the ultrasound signal, which is transmitted from the transmis-

sion/reception switching section 14, and performs processing such as amplification and conversion into a digital signal.

[0025] The phasing addition section 16 delays the ultrasound signal and adjusts a phase and then adds the ultrasound.

[0026] The signal processing section 17 performs coordinate conversion and interpolation processing on the ultrasound signal transmitted from the phasing addition section 16 and creates an ultrasound image as an image for display.

[0027] The displacement calculating section 21 measures displacement of the subject based on the ultrasound signal transmitted from the phasing addition section 16.

[0028] The elastic-image generating section 22 includes a distortion calculating section 23. The distortion calculating section 23 calculates, based on the displacement measured by the displacement calculating section 21, a distortion amount of a region of interest (ROI) (see an ROI 34 in Fig. 2 to Fig. 12) for elastic image display.

The elastic-image generating section 22 calculates a modulus of elasticity of the subject based on the distortion amount calculated by the distortion calculating section 23. The elastic-image generating section 22 calculates a modulus of elasticity for each of coordinates of the subject. Therefore, a calculation result is an elastic image in which moduli of elasticity are distributed on a two-dimensional coordinate. The generation of the elastic image by the elastic-image generating section 22 is performed, for example, every frame. One or more elastic images are generated. The elastic-image generating section 22 further calculates a distortion amount of the ROI 34 based on the displacement measured by the displacement calculating section 21 and performs coloring on pixels of the elastic images in which the distortion amount is equal to or larger than a predetermined value.

[0029] The memory section 24 is a storing section that temporarily stores the one or more elastic images generated by the elastic-image generating section 22.

[0030] The determination-region setting section 25 sets, according to a size of the ROI 34, a proper-image determination region 37 (see Fig. 4 to Fig. 12, etc.) for determining a proper image out of the one or more elastic images stored in the memory section 24.

[0031] The characteristic calculating section 26 calculates a region characteristic of the proper-image determination region 37 set by the determination-region setting section 25. Specifically, the characteristic calculating section 26 calculates, as the region characteristic, for example, at least one of an average of the displacement of the proper-image determination region 37 measured by the displacement calculating section 21, dispersion of the displacement, a deviation of the displacement and an average of elasticity information of the proper-image determination region 37 calculated by the elastic-image generating section 22, dispersion of the elasticity information, and a deviation of the elasticity information. The characteristic calculating section 26 may calculate, as

the region characteristic, at least one of the number of colored pixels and a total area of the colored pixels of the proper-image determination region 37, a ratio of the number of colored pixels to the number of pixels of the entire proper-image determination region 37, and a ratio of a total area of the colored pixels to an area of the entire proper-image determination region 37.

[0032] Note that a pressure detecting section for detecting pressure on an ultrasound transmission/reception surface for transmitting and receiving ultrasound may be further provided in the intra-body cavity probe 2, which is an ultrasound probe. The characteristic calculating section 26 may calculate, as the region characteristic, at least one of an average of pressure, a rate of change of the pressure, dispersion of the pressure, and a deviation of the pressure of the proper-image determination region 37 obtained based on a detection result of the pressure detecting section.

[0033] The proper-image determining section 27 determines based on the region characteristic calculated by the characteristic calculating section 26 whether the proper-image determination region 37 is a proper region. Further, when the proper-image determination region 37 is not the proper region, the proper-image determining section 27 causes the determination-region setting section 25 to set the proper-image determination region 37 again according to necessity. In this way, when at least one of the proper-image determination regions 37 set in the ROI 34 of the elastic image is the proper region, the proper-image determining section 27 determines that the elastic image in which the proper-image determination region 37 is set is a proper image.

[0034] The image display section 31 includes a display device such as a monitor and displays an image for display transmitted from the signal processing section 17. That is, in an ultrasound diagnosis mode, the image display section 31 displays an ultrasound image. In an elastic image observation mode, the image display section 31 displays an elastic image transmitted from the elastic-image generating section 22 or superimposes and displays the elastic image on the ultrasound image. When displaying the elastic image, the image display section 31 further superimposes and displays the proper-image determination region 37 transmitted from the proper-image determining section 27 on the elastic image according to necessity.

[0035] Fig. 2 is a diagram showing a state in which a region where a distortion amount is equal to or larger than a predetermined value in the ROI 34 is displayed. Fig. 3 is a diagram showing an example of a position of a displacement source with respect to the ROI 34.

[0036] As shown in the figure, on a screen 32 of the image display section 31, a probe image 33 showing a position of the intra-body cavity probe 2 itself as an image and the ROI 34 for elastic image display are displayed. A probe curvature radius R of the intra-body cavity probe 2 shown as the probe image 33 in Fig. 2 is, for example, 10 mm or less. The curvature radius R is relatively small.

Further, a center angle of the ROI 34 is, for example, approximately 180°.

[0037] In this case, in the ROI 34, a region 35 formed by pixels having a distortion amount equal to or larger than the predetermined value is displayed, for example, as shown in Fig. 2. The region 35 is generated as, for example, an image colored in a specific color by the elastic-image generating section 22, is displayed on the image display section 31, and can be easily distinguished from other portions. Therefore, in the example shown in Fig. 2, a colored region and an uncolored region are present in the ROI 34 of the elastic image.

[0038] When the user determines, viewing such an image, whether the image is an image suitable for a diagnosis and storage of the image, since the image is only partially colored with respect to the entire ROI 34, it is assumed that the user sometimes determines that the image is not the proper image.

[0039] However, when an ultrasound probe is the intra-body cavity probe 2 inserted into a body cavity and used, in order to generate an elastic image, displacement of an organism due to a beat or a pulsation is used. For example, when a displacement source 36 such as a pulsation source or a beat source is present in the position shown in Fig. 3, only the region 35 shown in Fig. 2 receives proper pressure and has a distortion amount equal to or larger than the predetermined value in the ROI 34. A distortion amount equal to or larger than the predetermined value does not occur in other regions. In this way, when the curvature radius R of the intra-body cavity probe 2 is small or when the center angle of the ROI 34 is wide, it cannot be expected that the entire ROI 34 is colored.

[0040] Therefore, in this case, it should be determined that the image shown in Fig. 2 is a proper image. Therefore, in the present embodiment, as explained below, a region for determining that an image is a proper image is set according to the size of the ROI 34 for elastic image display, a region characteristic in the set region is calculated, and it is determined according to the calculated characteristic whether the image is the proper image.

[0041] Action of generating an elastic image in such an ultrasound observation system is explained with reference to Fig. 13. Fig. 13 is a flowchart showing elastic image extraction processing in the ultrasound observation system.

[0042] When the ultrasound observation system is set in the elastic image observation mode while executing not-shown main processing, this elastic image extraction processing is started.

[0043] Then, first, the transmitting section 11 transmits an ultrasound signal to the intra-body cavity probe 2. Consequently, ultrasound is transmitted from the intra-body cavity probe 2 to the subject. The intra-body cavity probe 2 receives the ultrasound reflected by the subject, generates an ultrasound signal (an echo signal), and transmits the ultrasound signal to the ultrasound observation apparatus.

[0044] In the ultrasound observation apparatus, the re-

ceiving section 15 receives the ultrasound signal (the echo signal) via the transmission/reception switching section 14, the phasing addition section 16 and the displacement calculating section 21 perform processing, thereafter, the distortion calculating section 23 calculates a distortion amount of the ROI 34 for each of coordinate positions, and the elastic-image generating section 22 generates an elastic image based on the calculated distortion amount. Such acquisition of the elastic image is performed, for example, in frame units. Consequently, the ultrasound observation apparatus acquires one or more elastic images (step S1).

[0045] The ultrasound observation apparatus stores the one or more elastic images acquired in this way in the memory section 24 (step S2).

[0046] Thereafter, the ultrasound observation apparatus selects a first elastic image out of the elastic images stored in the memory section 24 (step S3).

[0047] Then, the determination-region setting section 25 determines whether a size of the ROI 34 of the selected elastic image (the size of the ROI 34 can be set by, for example, the user and, when the user setting is not performed, is set to a predetermined size) is equal to or smaller than a predetermined threshold (step S4). For example, a center angle of the ROI 34 is determined as the size of the ROI 34. The determination-region setting section 25 determines whether the center angle of the ROI 34 is equal to or smaller than a threshold. Note that the threshold used for the determination is desirably appropriately decided according to, for example, a size of the displacement source 36.

[0048] Fig. 4 is a diagram showing an example of the proper-image determination region 37 set when the center angle of the ROI 34 is larger than the predetermined threshold. Fig. 5 is a diagram showing an example of the proper-image determination region 37 set when the center angle of the ROI 34 is equal to or smaller than the predetermined threshold.

[0049] As explained above, when the center angle of the ROI 34 is large, pressure from the displacement source 36 is not easily appropriately applied to the entire ROI 34. However, when the center angle is small, appropriate pressure is considered to be applied to the entire ROI 34.

[0050] Therefore, in a first case in which it is determined in step S4 that the center angle of the ROI 34 for elastic image display is equal to or smaller than the predetermined threshold, the ultrasound observation apparatus performs single region processing (step S5). As explained with reference to Fig. 14, the single region processing is processing for setting the entire ROI 34 as the proper-image determination region 37.

[0051] On the other hand, in a second case in which it is determined in step S4 that the center angle of the ROI 34 is larger than the predetermined threshold, as explained in step S7, step S9, or step S10, a partial region, which is a part in the ROI 34, is set as the proper-image determination region 37.

[0052] As a specific example, when the threshold is set to 60°, when the center angle of the ROI 34 is approximately 180° (i.e., larger than 60°) as shown in Fig. 4, only the partial region in the ROI 34 is set as the proper-image determination region 37 and, when the center angle of the ROI 34 is approximately 30° (i.e., 60° or less) as shown in Fig. 5, the entire ROI 34 is set as the proper-image determination region 37.

[0053] When it is determined in step S4 that the center angle of the ROI 34 is larger than the predetermined threshold, further, the ultrasound observation apparatus determines whether the partial region is set to be sequentially scanned (step S6).

[0054] When it is determined that the sequential scan is set, the ultrasound observation apparatus performs sequential scan processing (step S7). As explained below with reference to Fig. 15, the sequential scan processing is processing in which the determination-region setting section 25 sequentially moves the partial region from a reference position by an offset amount at a time such that the entire ROI 34 is covered with the partial regions in all moving positions and sets each of the partial regions in the respective moving positions as the proper-image determination region 37.

[0055] When it is determined in step S6 that the sequential scan is not set, the ultrasound observation apparatus determines whether fixed-value division of the partial region is set (step S8).

[0056] When it is determined that the fixed-value division is set, the ultrasound observation apparatus performs fixed-value division processing (step S9). As explained below with reference to Fig. 16, the fixed-value division processing is processing in which the determination-region setting section 25 divides the entire ROI 34 into a plurality of partial regions and sets each of the partial regions as the proper-image determination region 37 and is processing for setting the number of divisions into partial regions of the entire ROI 34 based on a fixed value.

[0057] On the other hand, when it is determined in step S8 that the fixed-value division is not set, the ultrasound observation apparatus performs variable-value division processing (step S10). As explained below with reference to Fig. 17, the variable-value division processing is processing in which the determination-region setting section 25 divides the entire ROI 34 into a plurality of partial regions and sets each of the partial regions as the proper-image determination region 37 and is processing for changing the number of divisions into the partial regions of the entire ROI 34 between a lower limit value and an upper limit value until the proper-image determination region 37 determined as the proper region by the proper-image determining section 27 is found.

[0058] When the processing in any one of step S5, step S7, step S9, or step S10 is performed in this way, the ultrasound observation apparatus determines whether unprocessed other elastic images are present in the memory section 24 (step S11).

[0059] When it is determined that other elastic images are present, the ultrasound observation apparatus selects a next elastic image out of the unprocessed elastic images (step S12). Then, the ultrasound observation apparatus shifts to step S4 and repeatedly performs the processing explained above.

[0060] When it is determined in step S11 that unprocessed elastic images are absent, the ultrasound observation apparatus determines based on a processing result in step S5, step S7, step S9, or step S10 whether proper images are present among elastic images stored in the memory section 24 (step S13).

[0061] When it is determined in step S13 that proper images are present, the ultrasound observation apparatus extracts and displays all of the proper images on, for example, the image display section 31 (step S14). When it is determined that proper images are absent, the ultrasound observation apparatus directly returns from the elastic image extraction processing to not-shown main processing.

[0062] Fig. 14 is a flowchart showing single region processing.

[0063] When entering this processing in step S5 of Fig. 13, as explained above with reference to Fig. 5, the ultrasound observation apparatus sets the entire ROI 34 for elastic image display as the proper-image determination region 37 (step S21).

[0064] Subsequently, the ultrasound observation apparatus calculates a region characteristic of the proper-image determination region 37 (step S22). The ultrasound observation apparatus determines based on the calculated region characteristic whether the set proper-image determination region 37 is a proper region (step S23). The ultrasound observation apparatus returns from this processing to the processing shown in Fig. 13.

[0065] Fig. 15 is a flowchart showing the sequential scan processing.

[0066] When entering this processing in step S7 of Fig. 13, first, the ultrasound observation apparatus sets the proper-image determination region 37 at a predetermined angle (e.g., 60° same as the angle set as the threshold in step S4) as a reference position in the ROI 34 for elastic image display (step S31).

[0067] Subsequently, the ultrasound observation apparatus calculates a region characteristic of the proper-image determination region 37 (step S32) and determines based on the calculated region characteristic whether the set proper-image determination region 37 is a proper region (step S33).

[0068] The ultrasound observation apparatus determines whether regions not determined as to whether the regions are the proper region are present in the ROI 34 (step S34). When it is determined that undetermined regions are present, the ultrasound observation apparatus moves the proper-image determination region 37 by a predetermined offset amount (e.g., an offset angle 30°) in the ROI 34 and sets a new proper-image determination region 37 (step S35). The ultrasound observation appa-

ratus returns to step S32 and performs the processing explained above.

[0069] Consequently, as shown in Figs. 6 to 8, the sequential scan in which the proper-image determination region 37 moves by, for example, 30° at a time in order in the ROI 34 is performed. Fig. 6 is a diagram showing an example of a first position in sequentially scanning the proper-image determination region 37 in the ROI 34. Fig. 7 is a diagram showing an example of a second position in sequentially scanning the proper-image determination region 37 in the ROI 34. Fig. 8 is a diagram showing an example of a third position in sequentially scanning the proper-image determination region 37 in the ROI 34.

[0070] When the scan from one end to the other end of the ROI 34 is carried out in this way and it is determined in step S34 that undetermined regions are absent, the ultrasound observation apparatus returns from this processing to the processing shown in Fig. 13.

[0071] Fig. 16 is a flowchart showing the fixed-value division processing.

[0072] When entering this processing in step S9 in Fig. 13, first, the ultrasound observation apparatus divides the ROI 34 for elastic image display into partial regions based on a fixed value (step S41). The fixed value is, for example, a size of a partial region (an angle of the partial region) or the number of divisions.

[0073] For example, assuming that a center angle θ of the ROI 34 is larger than 60° (because, in the case of $\theta \leq 60^\circ$, the single region processing in step S5 is performed), the fixed value is set to an angle 60° of the partial region. In this case, when the center angle θ of the ROI 34 is, for example, 180° , as shown in Fig. 9, the entire ROI 34 is divided into three partial regions. The respective partial regions are set as first to third proper-image determination regions 37a to 37c in order. Fig. 9 is a diagram showing an example in which the proper-image determination region is divided by a fixed value in the ROI 34. In such a case in which the angle of the partial region is set to the fixed value, the number of divisions is different according to the center angle θ of the ROI 34 (e.g., when the center angle θ is 120° , the number of divisions is two).

[0074] When the fixed value is set to the number of divisions of three, as explained above, the ROI 34 is divided into three partial regions shown in Fig. 9 (as a desired division example, equally divided). In this case, the number of divisions is desirably given as a fixed value corresponding to a size of the center angle θ of the ROI 34. For example, when the center angle θ is $60^\circ < \theta \leq 120^\circ$, the fixed value is set to two. When the center angle θ is $120^\circ < \theta \leq 180^\circ$, the fixed value is set to three.

[0075] Subsequently, the ultrasound observation apparatus sets a first partial region among the divided partial regions as the proper-image determination region 37 (e.g., a first proper-image determination region 37a) (step S42), calculates a region characteristic of the proper-image determination region 37 (step S43), and determines

based on the calculated region characteristic whether the set proper-image determination region 37 is a proper region (step S44).

[0076] The ultrasound observation apparatus determines whether unprocessed partial regions (partial regions not determined as to whether the partial regions are the proper region) are present (step S45). When it is determined that unprocessed partial regions are present, the ultrasound observation apparatus sets a next partial region as a new proper-image determination region 37 (step S46). The ultrasound observation apparatus returns to S43 and performs the processing explained above.

[0077] When it is determined in step S45 that unprocessed partial regions are absent in this way, the ultrasound observation apparatus returns from this processing to the processing shown in Fig. 13.

[0078] Fig. 17 is a flowchart showing the variable-value division processing.

[0079] When entering this processing in step S10 in Fig. 13, first, the ultrasound observation apparatus sets, as an initial value, a lower limit value n_i of the number of divisions in a variable n indicating the number of divisions (step S51). The lower limit value n_i is, for example, 2 (when the number of divisions is one, the single region processing in step S5 is performed. Therefore, a suitable example of the lower limit value is 2 here).

[0080] Subsequently, the ultrasound observation apparatus divides (as a desirable division example, equally divides) the ROI 34 for elastic image display into n partial regions (step S52) and sets a first partial region among the divided partial regions in the proper-image determination region 37 (step S53).

[0081] Subsequently, the ultrasound observation apparatus calculates a region characteristic of the proper-image determination region 37 (step S54) and determines based on the calculated region characteristic whether the set proper-image determination region 37 is a proper region (step S55).

[0082] The ultrasound observation apparatus determines, according to whether it is determined in step S55 that the proper-image determination region 37 is the proper region, whether a processing target elastic image is a proper image (step S56).

[0083] When it is determined that the processing target elastic image is not a proper image, the ultrasound observation apparatus determines whether unprocessed partial regions (partial regions not determined as to whether the partial regions are a proper region) are present in the ROI 34 (step S57). When it is determined that unprocessed partial regions are present, the ultrasound observation apparatus sets the next partial region as a new proper-image determination region 37 (step S58). The ultrasound observation apparatus returns to step S54 and performs the processing explained above.

[0084] On the other hand, when it is determined in step S57 that unprocessed partial regions are absent, the ultrasound observation apparatus increases the variable

n indicating the number of divisions by 1 (step S59) and then determines whether n is larger than an upper limit value n_f of the number of divisions (step S60).

[0085] When it is determined that n is equal to or smaller than the upper limit value n_f of the number of divisions, the ultrasound observation apparatus returns to step S52 and performs, as explained above, processing based on the number of divisions n set anew.

[0086] Consequently, as shown in Fig. 10 to Fig. 12, variable-value division is performed in which the number of the proper-image determination regions 37 sequentially increases to two (37a and 37b) shown in Fig. 10, three (37a to 37c) shown in Fig. 11, and four (37a to 37d) shown in Fig. 12. Fig. 10 is a diagram showing a first division example in dividing the proper-image determination region 37 by a variable value in the ROI 34. Fig. 11 is a diagram showing a second division example in dividing the proper-image determination region 37 by a variable value in the ROI 34. Fig. 12 is a diagram showing a third division example in dividing the proper-image determination region 37 by a variable value in the ROI 34.

[0087] When it is determined in step S60 that n is larger than the upper limit value n_f or it is determined in step S56 that the processing target elastic image is a proper image, the ultrasound observation apparatus returns from this processing to the processing shown in Fig. 13.

[0088] Note that the number of divisions n is changed from the lower limit value n_i to the upper limit value n_f . However, the number of divisions n may be changed from the upper limit value n_f to the lower limit value n_i . The change of the number of divisions n is not limited to these examples. The number of divisions n may be changed in appropriate order between a value equal to or larger than the lower limit value n_i and a value equal to or smaller than the upper limit value n_f .

[0089] Note that (1) the threshold compared with the size of the ROI 34 in step S4 of Fig. 13, (2) the angle of the proper-image determination region 37 in step S31 and the offset amount in step S35 of Fig. 15, (3) the fixed value in step S41 of Fig. 16, and (4) the lower limit value n_i in step S51 and the upper limit value n_f in step S60 of Fig. 17 may be automatically set based on design values or a user may manually set the values. In this case, concerning (2), (3), and (4), the determination-region setting section 25, the proper-image determining section 27, or the like may store, in advance, a table for giving predetermined values corresponding to the size of the center angle of the ROI 34. The ultrasound observation apparatus may determine the respective values referring to the table based on the size of the center angle of the ROI 34 set by the user or the like.

[0090] In the above explanation, which processing of the single region processing in step S5, the sequential scan of step S7, the fixed-value division of step S9, and the variable-value division of step S10 is performed is automatically set. However, the user may manually select the processing.

[0091] Further, in the respective kinds of processing

explained above, when it is determined that the proper-image determination region 37 is a proper region, the proper-image determining section 27 may further superimposes a region determined as a proper region on the elastic image, cause the image display section 31 to display the region, and clearly indicate the region to the user. In this case, the proper-image determining section 27 generates a signal for superimposing and displaying the proper-image determination region 37 determined as proper on the elastic image and transmits the signal to the image display section 31.

[0092] In the above explanation, the intra-body cavity probe 2 is explained as an example. However, the present invention is not limited to this. The ultrasound probe may be an external ultrasound probe. When the ultrasound probe is the external ultrasound probe, specifically, a linear ultrasound probe, the threshold compared with the size of the ROI 34 in step S4 of Fig. 13 only has to be, for example, length in a linear scan direction.

[0093] According to such a first embodiment, the proper-image determination region 37 is set according to the size of the ROI 34. It is determined based on the region characteristic of the proper-image determination region 37 whether the elastic image is a proper image. Therefore, it is possible to automatically extract a proper image without depending on the size of the ROI 34.

[0094] When the size of the ROI 34 is equal to or smaller than the threshold, the entire ROI 34 is set as the proper-image determination region 37. When the size of the ROI 34 is larger than the threshold, the partial region is set as the proper-image determination region 37. Therefore, it is possible to perform appropriate determination according to the size of the displacement source 36.

[0095] Further, when the sequential scan is performed, it is possible to perform appropriate determination without depending on the position of the displacement source 36 with respect to the ROI 34.

[0096] When the fixed-value division is performed, it is possible to perform appropriate determination not depending on the position of the displacement source 36 without requiring the processing for moving the proper-image determination region 37.

[0097] On the other hand, when the variable-value division is performed, it is possible to cope with a change in a size of a region that receives pressure from the displacement source 36.

[0098] When at least one of the average, the dispersion, and the deviation of the displacement and the average, the dispersion, and the deviation of the elasticity information of the proper-image determination region 37 is calculated as the region characteristic, it is possible to perform appropriate determination corresponding to the displacement or the elasticity information.

[0099] Further, when at least one of the number of colored pixels and the total area of the colored pixels of the proper-image determination region 37, the ratio of

the number of colored pixels to the number of pixels of the entire proper-image determination region 37, and the ratio of the total area of the colored pixels to the area of the entire proper-image determination region 37 is calculated as the region characteristic, it is possible to perform appropriate determination using the colored pixels.

[0100] When at least one of the average of the pressure, the rate of change of the pressure, the dispersion of the pressure, and the deviation of the pressure of the proper-image determination region 37 is calculated as the region characteristic, it is possible to perform appropriate determination corresponding to the pressure.

[0101] In addition, the proper-image determination region 37 determined as proper is superimposed and displayed on the elastic image. Therefore, the user can easily check the proper-image determination region 37, based on which the elastic image is determined as the proper image.

[0102] Note that, in the above explanation, the ultrasound observation system including the ultrasound observation apparatus is mainly explained. However, the present invention may be an actuation method for actuating the ultrasound observation apparatus or the ultrasound observation system as explained above, a processing program for causing a computer to actuate the ultrasound observation apparatus or the ultrasound observation system as explained above, a nontransitory recording medium that records the processing program and is readable by the computer, and the like.

[0103] The present invention is not limited to the embodiment per se. In an implementation stage, the constituent elements can be modified and embodied in a range not departing from the spirit of the present invention. Forms of various inventions can be formed by appropriate combinations of the plurality of constituent elements disclosed in the embodiment. For example, several constituent elements can be deleted from all the constituent elements described in the embodiments. Further, the constituent elements described in different embodiments may be combined as appropriate. In this way, it goes without saying that various modifications and applications are possible in a range not departing from the spirit of the invention.

[0104] This application is based upon and claims the benefit of priority from Japanese Patent Application No. 2014-170752 filed in Japan on August 25, 2014, the disclosed contents of which are incorporated in the specification, the claims, and the drawings of this application.

Claims

1. An ultrasound observation apparatus that generates an ultrasound image based on an ultrasound signal generated from ultrasound transmitted to a subject and reflected, the ultrasound observation apparatus comprising:

- a transmitting section that transmits a driving signal for generating the ultrasound transmitted to the subject;
 a receiving section that receives the ultrasound signal generated from the ultrasound reflected by the subject;
 a displacement calculating section that measures displacement of the subject based on the ultrasound signal received by the receiving section;
 an elastic-image generating section that generates an elastic image based on the displacement measured by the displacement calculating section;
 a storing section that stores one or more of the elastic images generated by the elastic-image generating section;
 a determination-region setting section that sets, according to a size of an ROI, which is a region of interest, a proper-image determination region for determining a proper image out of the one or more elastic images stored in the storing section;
 a characteristic calculating section that calculates a region characteristic of the proper-image determination region; and
 a proper-image determining section that determines based on the region characteristic whether the elastic image in which the proper-image determination region is set is the proper image.
2. The ultrasound observation apparatus according to claim 1, wherein the determination-region setting section sets the entire ROI as the proper-image determination region in a first case in which the size of the ROI is equal to or smaller than a threshold and sets a partial region, which is a part of the ROI, as the proper-image determination region in a second case in which the size of the ROI is larger than the threshold.
 3. The ultrasound observation apparatus according to claim 2, wherein, in the second case, the determination-region setting section sequentially moves the partial region from a reference position by an offset amount at a time such that the entire ROI is covered with the partial regions in all moving positions and sets each of the partial regions in the respective moving positions as the proper-image determination region.
 4. The ultrasound observation apparatus according to claim 2, wherein, in the second case, the determination-region setting section divides the entire ROI into the partial region in plurality and sets each of the partial regions as the proper-image determination region.
 5. The ultrasound observation apparatus according to claim 4, wherein a number of divisions into the partial regions of the entire ROI is set based on a fixed value.
 6. The ultrasound observation apparatus according to claim 4, wherein the determination-region setting section changes a number of divisions into the partial regions of the entire ROI between a value equal to or larger than a lower limit value and a value equal to or smaller than an upper limit value until the proper-image determination region determined as proper by the proper-image determining section is found.
 7. The ultrasound observation apparatus according to claim 1, wherein the proper-image determining section determines based on the region characteristic whether the proper-image determination region is proper and, when it is determined that one or more of the proper-image determination region is proper, determines that the elastic image in which the proper-image determination region is set is a proper image.
 8. The ultrasound observation apparatus according to claim 1, wherein the characteristic calculating section calculates, as the region characteristic, at least one of an average of displacement of the proper-image determination region measured by the displacement calculating section, dispersion of the displacement, and a deviation of the displacement and an average of elasticity information of the proper-image determination region calculated by the elastic-image generating section, dispersion of the elasticity information, and a deviation of the elasticity information.
 9. The ultrasound observation apparatus according to claim 1, wherein the elastic-image generating section further calculates a distortion amount of the ROI based on displacement measured by the displacement calculating section and performs coloring on pixels of the elastic image, the distortion amount of which is equal to or larger than a predetermined value, and the characteristic calculating section calculates, as the region characteristic, at least one of a number of the colored pixels and a total area of the colored pixels of the proper-image determination region, a ratio of the number of colored pixels to a number of pixels of the entire proper-image determination region, and a ratio of a total area of the colored pixels to an entire area of the proper-image determination region.
 10. The ultrasound observation apparatus according to claim 1, wherein the proper-image determining section further generates a signal for superimposing and displaying the proper-image determination region

determined as proper on the elastic image.

11. An ultrasound observation system comprising:

the ultrasound observation apparatus according to claim 1; and
an ultrasound probe that receives the driving signal transmitted from the transmitting section, transmits the ultrasound to the subject, receives the ultrasound reflected by the subject, generates the ultrasound signal, and transmits the ultrasound signal to the receiving section.

12. The ultrasound observation system according to claim 11, wherein the ultrasound probe further comprises a pressure detecting section for detecting pressure on an ultrasound transmission/reception surface for transmitting and receiving the ultrasound, and
the characteristic calculating section calculates, as the region characteristic, at least one of an average of pressure, a rate of change of the pressure, dispersion of the pressure, and a deviation of the pressure of the proper-image determination region obtained based on a detection result of the pressure detecting section.

13. An actuation method for an ultrasound observation apparatus that generates an ultrasound image based on an ultrasound signal generated from ultrasound transmitted to a subject and reflected, the actuation method for the ultrasound observation apparatus comprising:

a step in which a transmitting section transmits a driving signal for generating the ultrasound transmitted to the subject;
a step in which a receiving section receives the ultrasound signal generated from the ultrasound reflected by the subject;
a step in which a displacement calculating section measures displacement of the subject based on the ultrasound signal received by the receiving section;
a step in which an elastic-image generating section generates an elastic image based on the displacement measured by the displacement calculating section;
a step in which a storing section stores one or more of the elastic images generated by the elastic-image generating section;
a step in which a determination-region setting section sets, according to a size of an ROI, which is a region of interest, a proper-image determination region for determining a proper image out of the one or more elastic images stored in the storing section;
a step in which a characteristic calculating sec-

tion calculates a region characteristic of the proper-image determination region; and
a step in which a proper-image determining section determines based on the region characteristic whether the elastic image in which the proper-image determination region is set is the proper image.

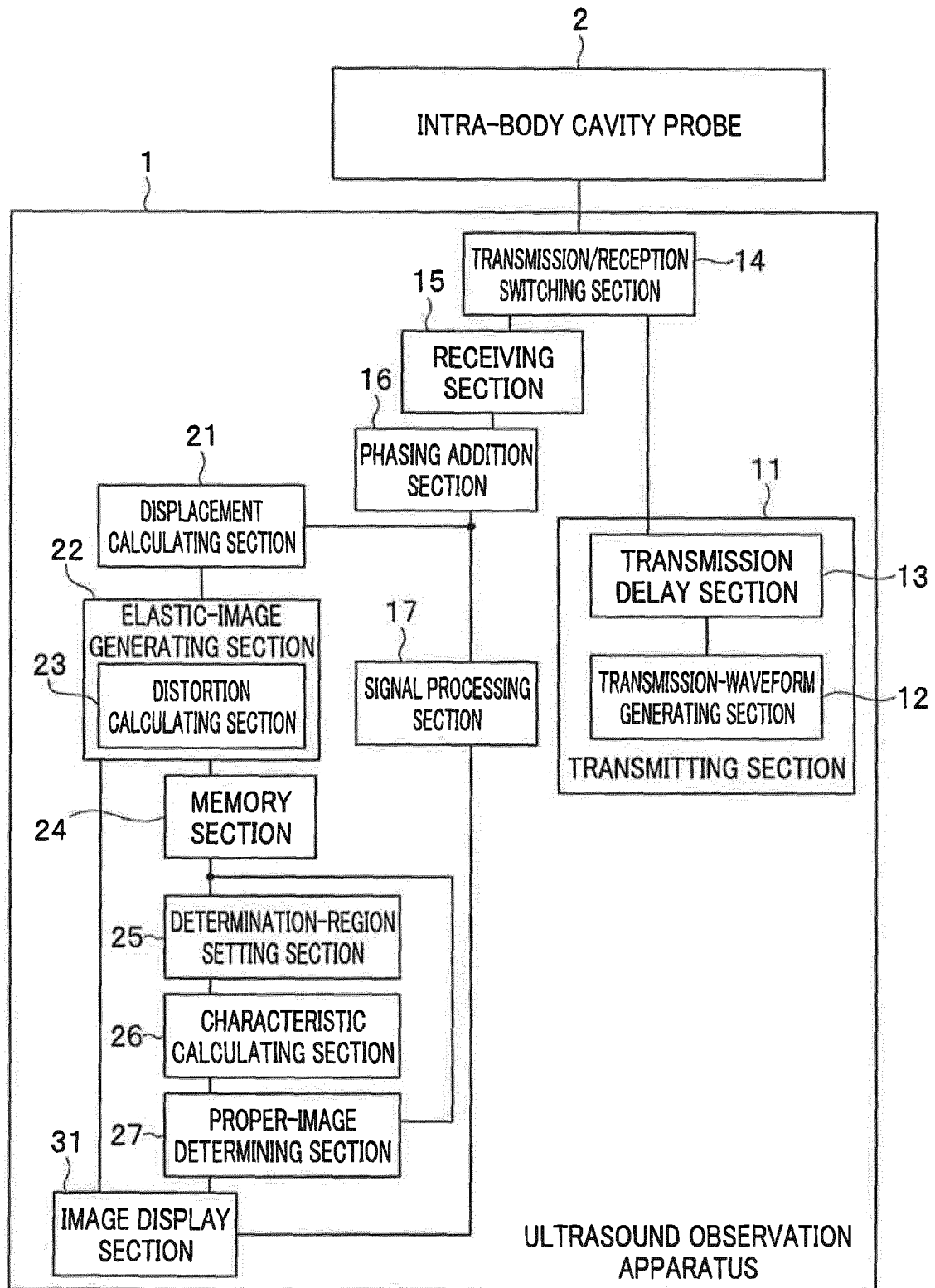
FIG. 1

FIG. 2

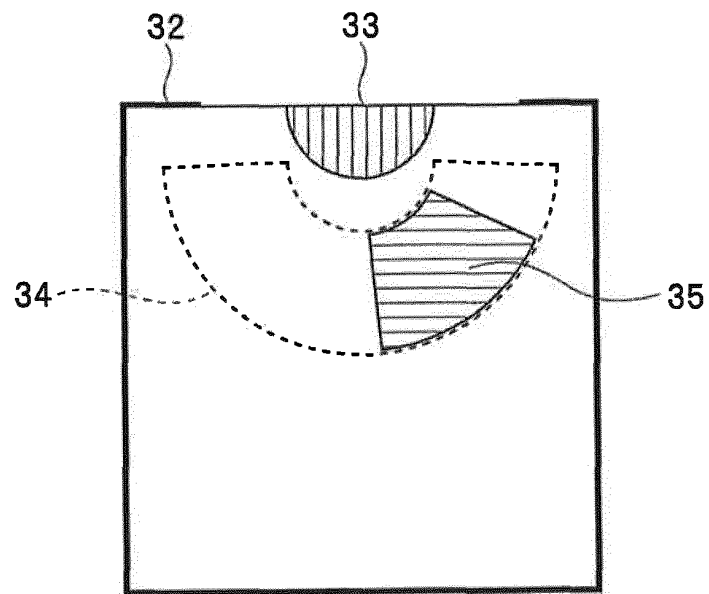


FIG. 3

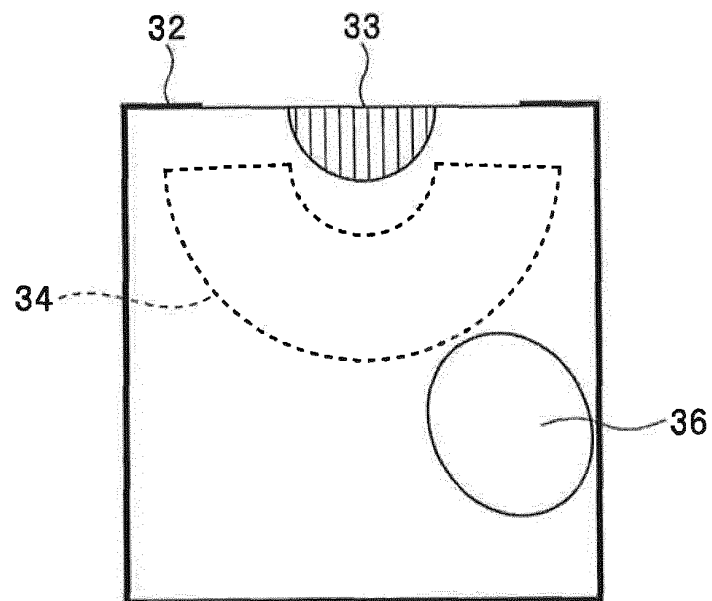


FIG. 4

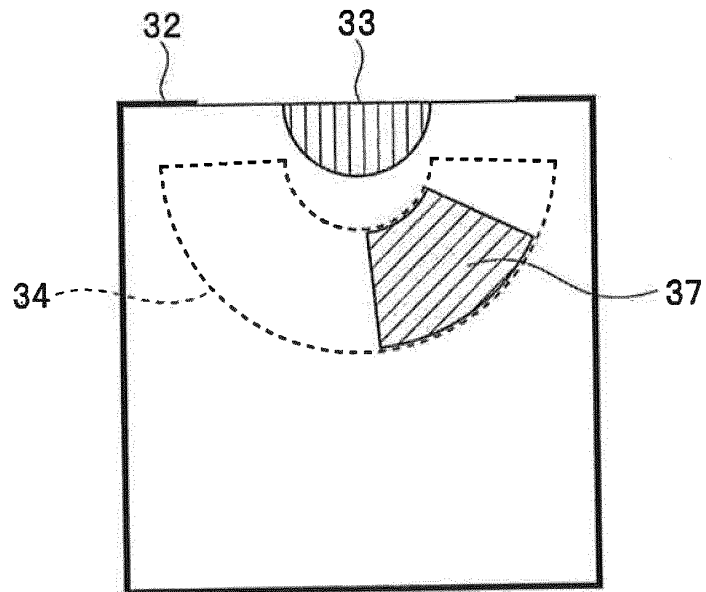


FIG. 5

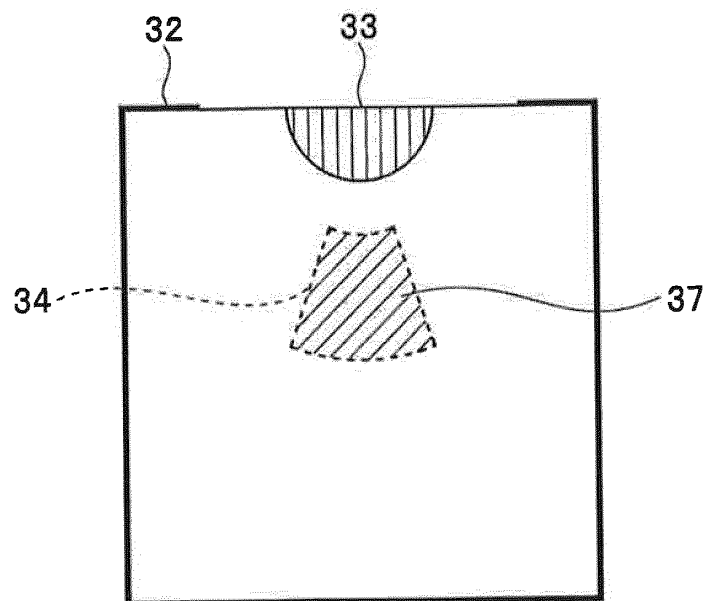


FIG. 6

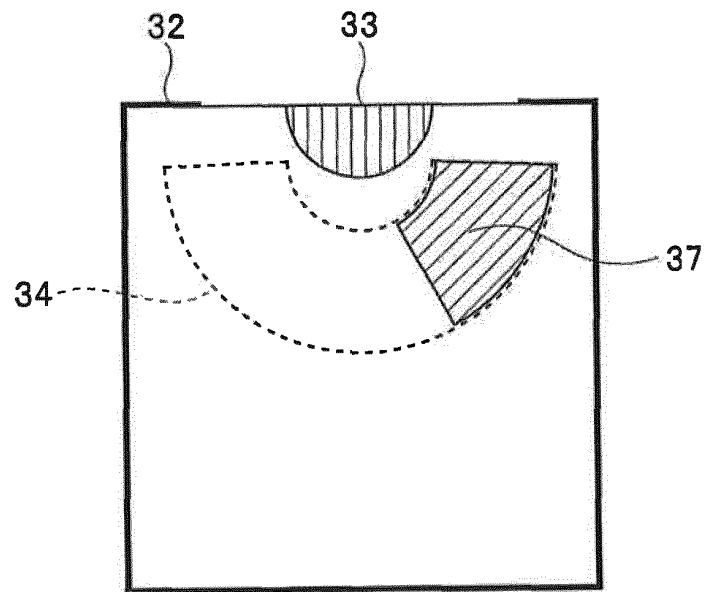


FIG. 7

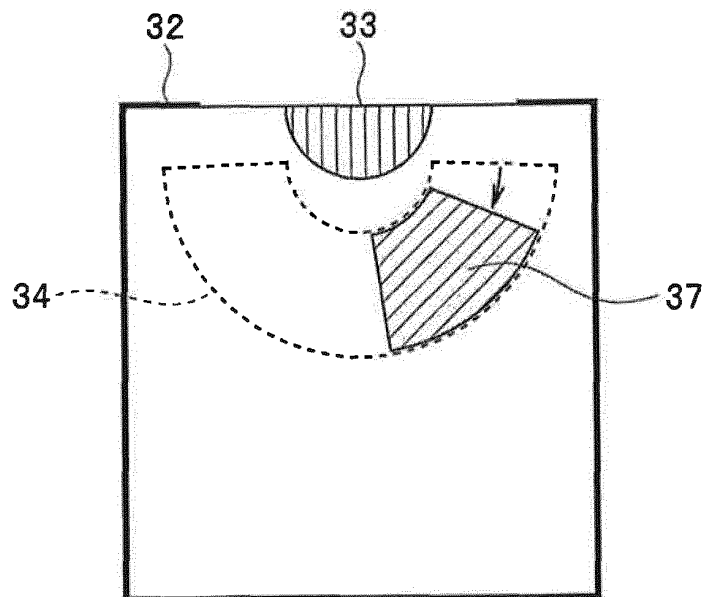


FIG. 8

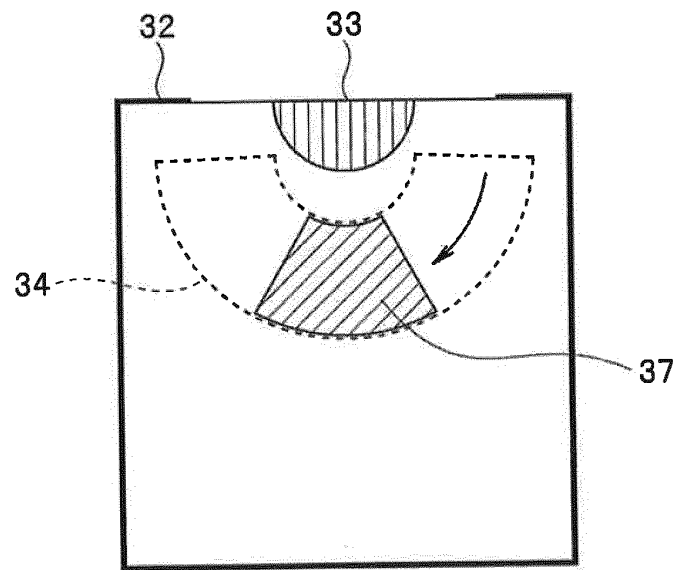


FIG. 9

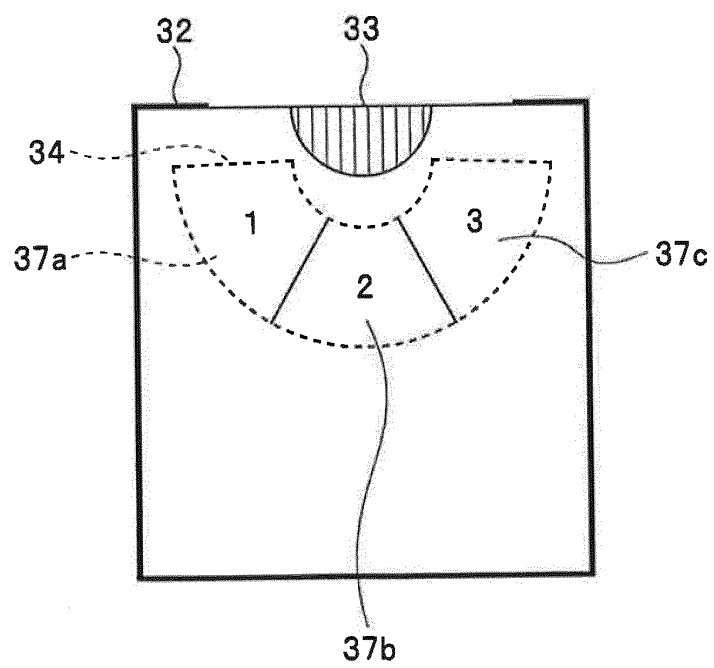


FIG. 10

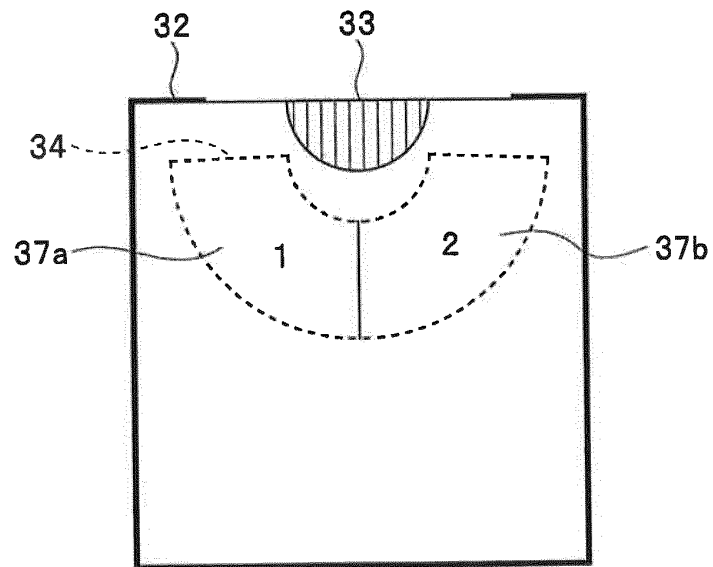


FIG. 11

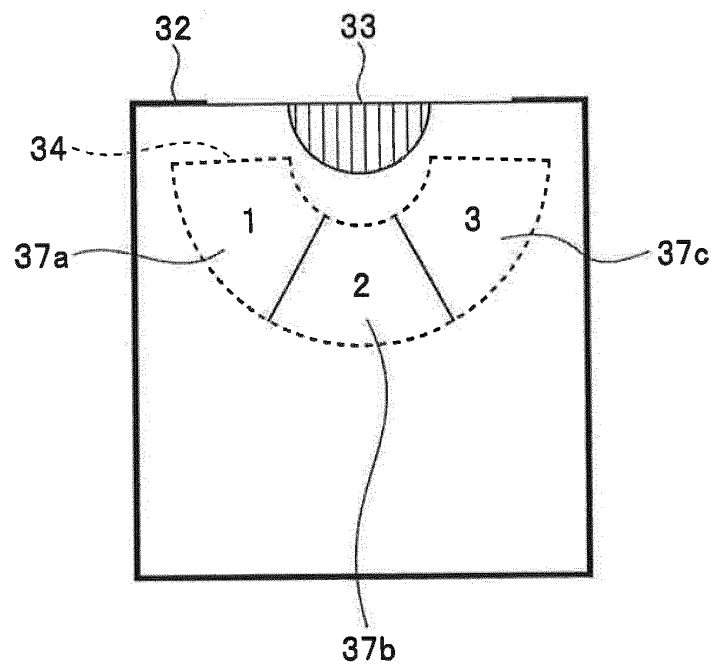


FIG. 12

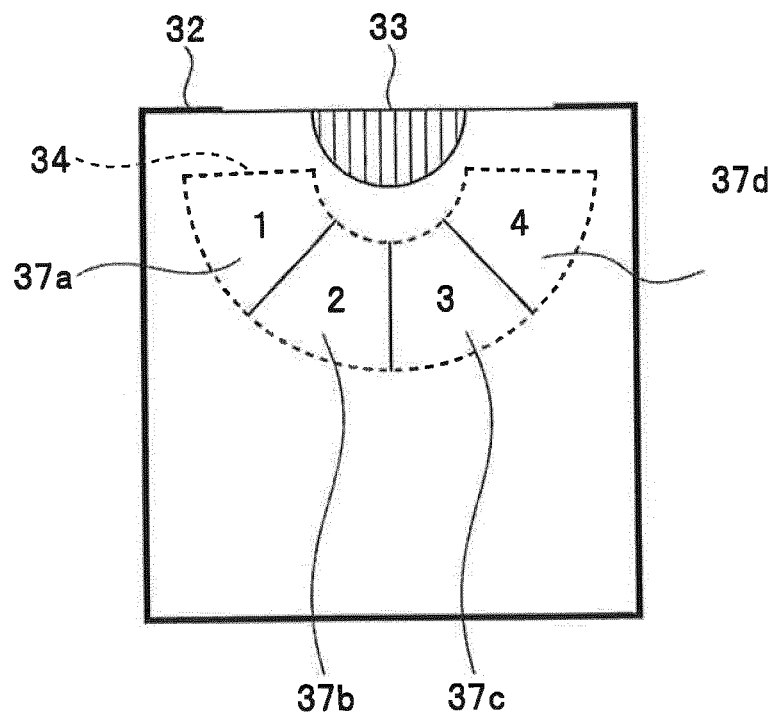


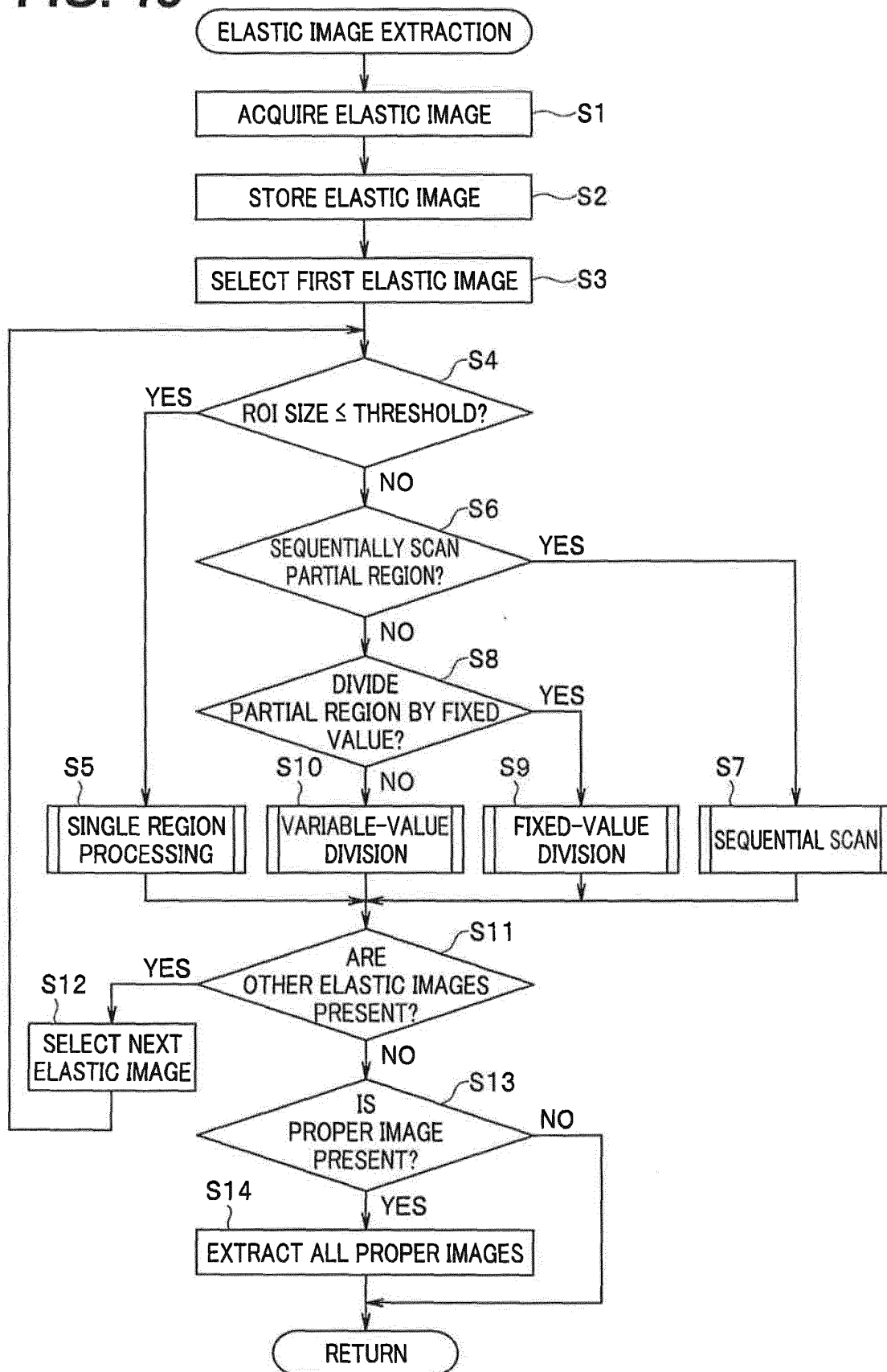
FIG. 13

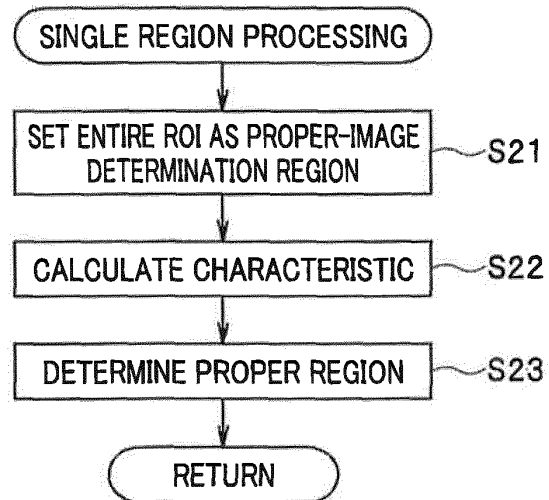
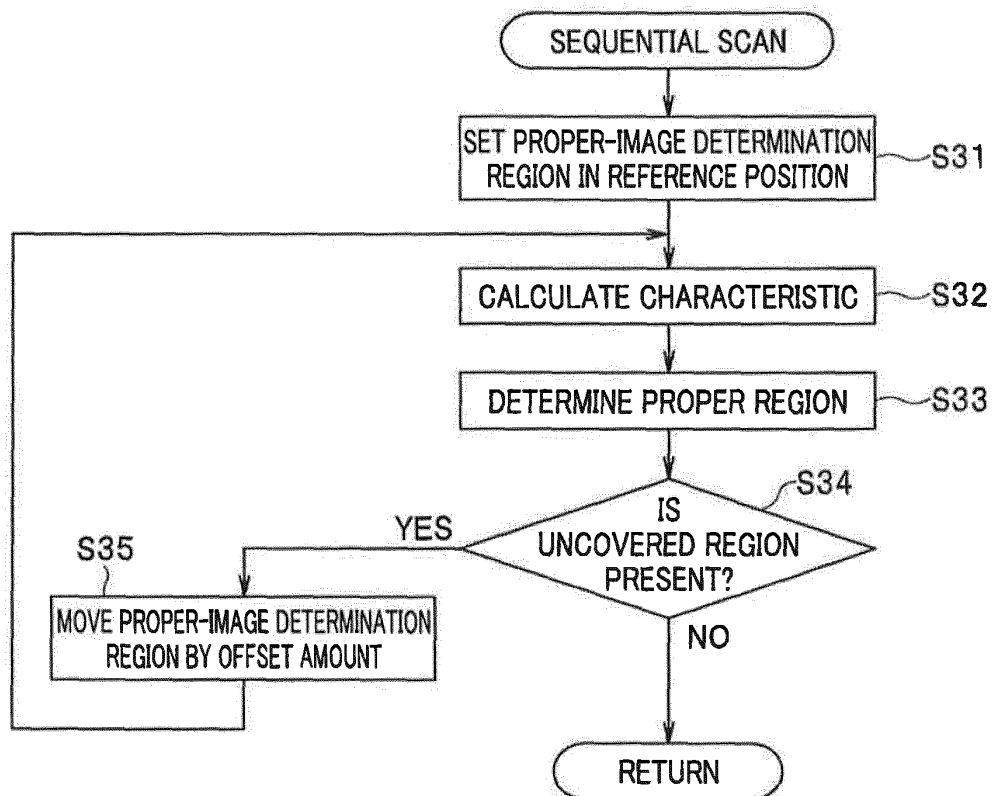
FIG. 14**FIG. 15**

FIG. 16

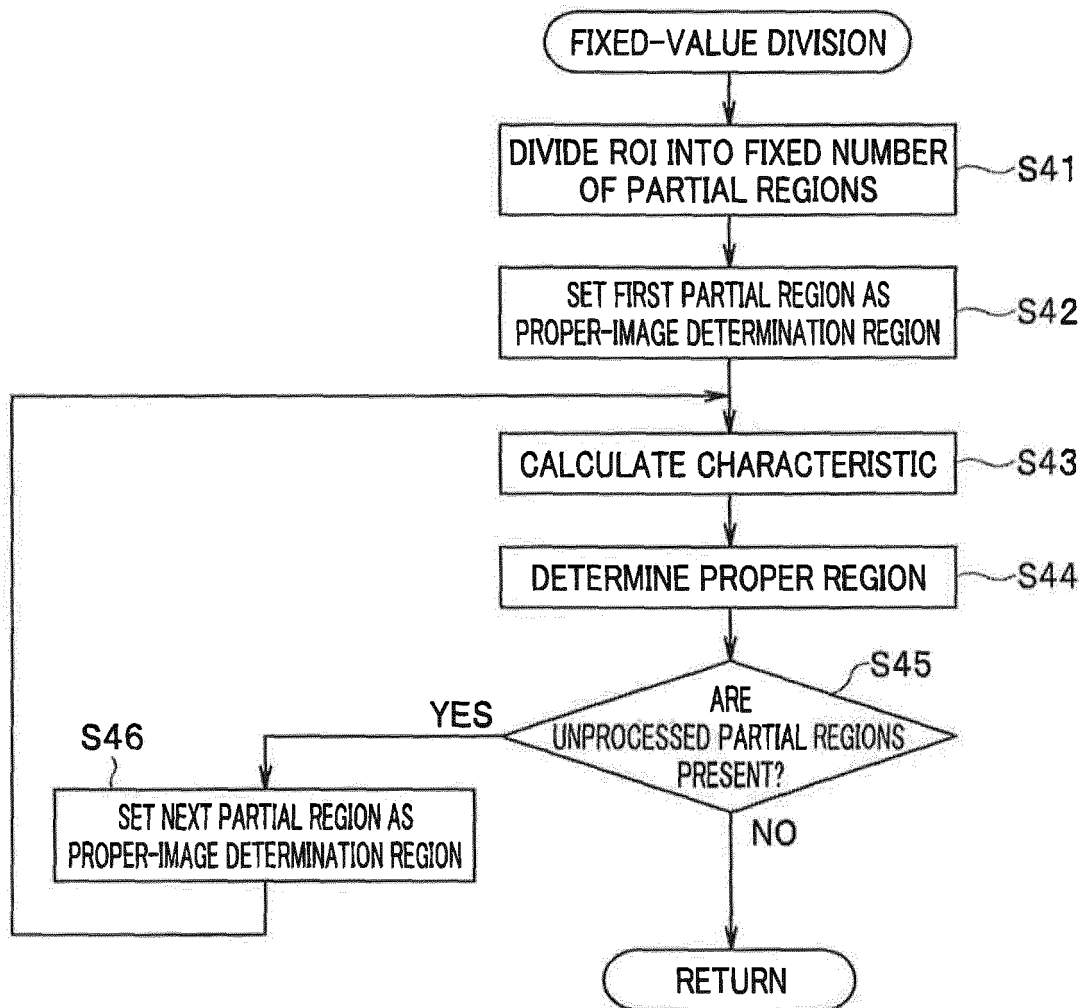
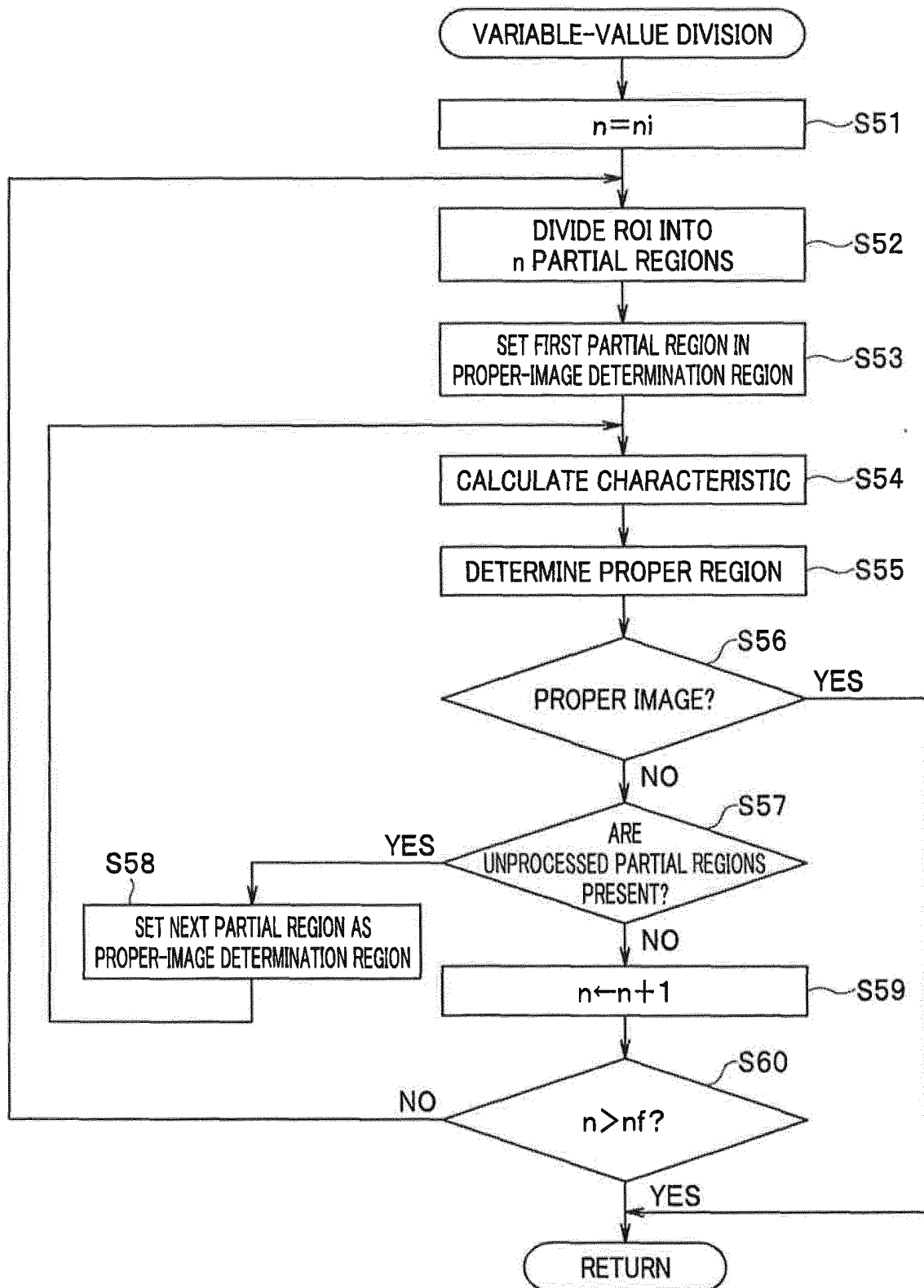


FIG. 17



INTERNATIONAL SEARCH REPORT

International application No.

PCT/JP2015/057196

A. CLASSIFICATION OF SUBJECT MATTER

A61B8/12(2006.01)i, A61B8/08(2006.01)i

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

A61B8/00-8/15

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Jitsuyo Shinan Koho 1922-1996 Jitsuyo Shinan Toroku Koho 1996-2015

Kokai Jitsuyo Shinan Koho 1971-2015 Toroku Jitsuyo Shinan Koho 1994-2015

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	JP 2010-119630 A (GE Medical Systems Global Technology Company, L.L.C.), 03 June 2010 (03.06.2010), entire text; all drawings (Family: none)	1-13
A	JP 2012-213545 A (Hitachi Medical Corp.), 08 November 2012 (08.11.2012), entire text; all drawings (Family: none)	1-13
A	WO 2011/010626 A1 (Hitachi Medical Corp.), 27 January 2011 (27.01.2011), entire text; all drawings & US 2012/0253195 A1	1-13

☒ Further documents are listed in the continuation of Box C.
 ☐ See patent family annex.

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"P" document published prior to the international filing date but later than the priority date claimed

"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

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"&" document member of the same patent family

Date of the actual completion of the international search

08 May 2015 (08.05.15)

Date of mailing of the international search report

19 May 2015 (19.05.15)

Name and mailing address of the ISA/

Japan Patent Office

3-4-3, Kasumigaseki, Chiyoda-ku,

Tokyo 100-8915, Japan

Authorized officer

Telephone No.

INTERNATIONAL SEARCH REPORT

International application No.

PCT/JP2015/057196

C (Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	JP 2005-118152 A (Hitachi Medical Corp.), 12 May 2005 (12.05.2005), entire text; all drawings & WO 2004/105615 A1 & EP 1629777 A1 & JP 4455003 B2	1-13

Form PCT/ISA/210 (continuation of second sheet) (July 2009)

REFERENCES CITED IN THE DESCRIPTION

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Patent documents cited in the description

- WO 2011010626 A [0005] [0008]
- JP 2012213545 A [0006] [0009]
- JP 2005118152 A [0007] [0009]
- JP 2014170752 A [0104]

专利名称(译)	超声波观察装置，超声波观察系统以及超声波观察装置的操作方法		
公开(公告)号	EP3020339A4	公开(公告)日	2017-04-05
申请号	EP2015808067	申请日	2015-03-11
[标]申请(专利权)人(译)	奥林巴斯株式会社		
申请(专利权)人(译)	OLYMPUS CORPORATION		
当前申请(专利权)人(译)	奥林巴斯公司		
[标]发明人	MIYAKE TATSUYA		
发明人	MIYAKE, TATSUYA		
IPC分类号	A61B8/12 A61B8/08		
CPC分类号	A61B8/5207 A61B8/08 A61B8/12 A61B8/4444 A61B8/461 A61B8/485		
优先权	2014170752 2014-08-25 JP		
其他公开文献	EP3020339A1		
外部链接	Espacenet		

摘要(译)

一种超声波观察装置 (1)，包括基于超声波信号测量被检体的位移的位移计算部分 (21)，基于测量的位移产生弹性图像的弹性图像产生部分 (22)，存储部分 (24) 存储生成的一个或多个弹性图像，确定区域设置部分 (25)，其根据ROI的大小设置用于在弹性图像中进行适当图像确定的适当图像确定区域，特征计算部分 (26) 计算适当图像确定区域的区域特性，以及基于区域特征确定弹性图像是否是适当图像的适当图像确定部分 (27)。