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(54) **SPATIALLY-FINE SHEAR WAVE DISPERSION ULTRASOUND VIBROMETRY SAMPLING**

ULTRASCHALL-VIROMETRIEABTASTUNG MIT RÄUMLICH FEINER SCHERWELLENDISPERSION

ÉCHANTILLONNAGE PRÉCIS DANS L'ESPACE PAR VIBROMÉTRIE ULTRASONORE À DISPERSION DES ONDES DE CISAILLEMENT

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(56) References cited:
WO-A1-2006/113445 WO-A1-2008/139245
WO-A2-2007/144520 US-A- 5 685 308
US-A1- 2002 143 253 US-A1- 2004 167 403
US-A1- 2006 122 506 US-A1- 2009 069 693

- **BERCOFF J ET AL: "SUPERSONIC SHEAR IMAGING: A NEW TECHNIQUE FOR SOFT TISSUE ELASTICITY MAPPING" IEEE TRANSACTIONS ON ULTRASONICS, FERROELECTRICS AND FREQUENCY CONTROL, IEEE, US, vol. 51, no. 4, 1 April 2004 (2004-04-01), pages 396-409, XP001218171 ISSN: 0885-3010 DOI: DOI:10.1109/TUFFC.2004.1295425**
- **DEFFIEUX T ET AL: "Shear Wave Spectroscopy for In Vivo Quantification of Human Soft Tissues Visco-Elasticity" IEEE TRANSACTIONS ON MEDICAL IMAGING, IEEE SERVICE CENTER, PISCATAWAY, NJ, US, vol. 28, no. 3, 1 March 2009 (2009-03-01), pages 313-322, XP011247217 ISSN: 0278-0062**
- **BOUCHARD R ET AL: "Image quality, tissue heating, and frame rate trade-offs in acoustic radiation force impulse imaging" IEEE TRANSACTIONS ON ULTRASONICS, FERROELECTRICS AND FREQUENCY CONTROL, IEEE, US LNKD- DOI:10.1109/TUFFC.2009.1006, vol. 56, no. 1, 1 January 2009 (2009-01-01), pages 63-76, XP011267404 ISSN: 0885-3010**

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DescriptionFIELD OF THE INVENTION

5 **[0001]** The present invention is directed to measuring a shear wave and, more particularly, to doing so by Shear Wave Dispersion Ultrasound Vibrometry (SDUV).

BACKGROUND OF THE INVENTION

10 **[0002]** Mechanical changes in living tissue correlate with pathological changes. As between healthy and pathological tissue, the shear elastic modulus (stiffness) and viscosity can vary significantly. With the advent of ultrasound elasticity imaging development over the past decade, many clinical studies have shown that tissue viscoelastic properties provide useful information to physicians for better cancer diagnosis and therapy assessment.

15 **[0003]** Shear Wave Dispersion Ultrasound Vibrometry (SDUV) is an acoustic radiation force based technique that measures tissue shear elasticity and viscosity by characterizing shear wave speed dispersion, i.e., by frequency. An application of this technique is the non-invasive measurement of liver stiffness to stage liver fibrosis and cirrhosis.

20 **[0004]** Interrogation by ultrasound, for purposes of medical imaging, often makes use of longitudinal waves. In body tissue, the ultrasound propagates in wave form. In effect, particles all along the propagation path vibrate, in place, back and forth, and the vibration occurs in the direction of propagation. The vibrations create compressions and rarefactions. These are modeled as the peaks and valleys of a sinusoid. Energy is conveyed to the target and back by means of the oscillatory particle movements.

[0005] An ultrasound shear (or transverse) wave, by contrast, is characterized by back and forth in-place movement that is perpendicular to the direction of propagation. Oscillation one way creates the peaks, and the other way creates the valleys.

25 **[0006]** Performing SDUV entails issuing a series of focused longitudinal-wave push pulses. They are high intensity, narrow bandwidth signals which are fired with a repetition rate of (say) 100Hz. After several of these pulses are fired, each laterally coinciding and in the same direction, they establish a shear wave which propagates out from the focus and in a direction perpendicular to that of the push pulses. The focal depth has been selected so that the shear wave travels through a region of interest (ROI).

30 **[0007]** A longitudinal-wave tracking pulse is issued to the ROI to assess, at the sampling point, the amplitude of the shear wave. This measurement is used in estimating the phase of the shear wave at the sampled location.

[0008] To sample another location, another push pulse issues to the same pushing focus, followed by a tracking pulse to that location. This second cycle is needed, because the difference in phase between two points is used in the determining of elasticity and viscosity.

35 **[0009]** Shear waves with frequencies of typically 100 Hz and harmonics (200 Hz, 300 Hz, 400 Hz), i.e., components (or "monochromatic shear waves"), are present because the envelope of the pushing pulse is a square wave. The speed estimations at the different frequencies are used in deriving tissue shear elasticity and viscosity.

40 **[0010]** US2004/0167403 discloses a Shear Wave Ultrasound examination method comprising, the steps of forming, from a single tracking pulse, a plurality of receive lines and processing said receive lines via a parallel processing techniques for making measurements of a monochromatic shear wave. Document XP1218171 teaches the use of plane wave as tracking pulse for Supersonic Shear Wave Imaging.

SUMMARY OF THE INVENTION

45 **[0011]** The invention is defined in the independent claims 1,6 and 10. Preferred embodiments are defined in the dependent claims. Shortcomings of the prior art of record are addressed hereinafter.

50 **[0012]** One main challenge associated with detecting radiation-force-induced shear waves using SDUV is the relatively low amplitude vibration. Axial displacement is on the order of 10 μm . The vibration amplitudes are therefore susceptible to noise. System electronic noise and patient motion such as cardiac or respiratory motion will contribute significant noise to shear wave displacement estimation.

[0013] In addition, fast imaging is required to detect the shear waves. Vibrations at up to 400 Hz must be recorded, because higher frequency shear waves are attenuated by the medium. Accordingly, to safely exceed the Nyquist threshold, each spatial location must be sampled at greater than 1000 Hz to prevent aliasing. Since the tracking pulse repetition frequency is limited by the speed of sound in tissue and the depth of the ROI, this limits the number of spatial locations that can be sampled, using conventional non-multiline detection sequences.

55 **[0014]** Using a multiline beamformer, as proposed hereinafter allows for finer spatial sampling of the displacement field, and/or spatial sampling in both the elevation and lateral imaging planes (when using 2D arrays vs. conventional 1D arrays). Since more information is extracted from each of the detection pulses, the robustness of the elasticity

measures from SDUV is increased. As an added benefit, the total time spent in the procedure can therefore be shortened. This is advantageous from a patient convenience standpoint, and for reducing the potential impact of thermal effects from the repeated delivery of pushes to the excitation point. In addition, the increased pace of radio frequency (RF) data acquisition makes way for the employment of other shear wave imaging/quantification techniques that require high spatial resolution with high speed.

5 [0015] In one version of the present invention, shear wave dispersion ultrasound vibrometry (SDUV) is performed by forming, from a single tracking pulse, in-parallel-directed receive lines for making measurements of a monochromatic shear wave.

10 [0016] As an aspect, from at least one other tracking pulse, the forming is executed so as to overlap resulting receive lines to increase depth of field.

[0017] More particularly, in some embodiments, the increasing entails combining from among the overlapped receive lines to create at least one reconstructed A-line.

[0018] Related other possible aspects involve forming, from differently-timed ones of the at least one other tracking pulse, respective pluralities of reconstructed A-lines created by the combining.

15 [0019] As a specific embodiment, making measurements includes making amplitude measurements of the monochromatic shear wave.

[0020] What is proposed herein is implementable as an apparatus for performing shear wave dispersion ultrasound vibrometry (SDUV), configured for forming, from a single tracking pulse, a plurality of in-parallel-directed receive lines for making measurements of the monochromatic shear wave.

20 [0021] Such apparatus may be characterized in that the tracking pulse, and at least one laterally-offset tracking pulse, are focused to a common depth, the apparatus being configured for, based on echo data from the pulses focused to that depth, reconstructing a shallower transmit focus.

[0022] Or, in an alternative or supplemental aspect, the apparatus is configured for such forming for at least one other tracking pulse and so as to overlap receive lines, and further configured for interpolating pulse firing times, to, in determining phase difference, correct for intersample wave propagation.

25 [0023] In one form, a computer software product for performing shear wave dispersion ultrasound vibrometry (SDUV) includes a computer readable medium embodying a computer program that includes instructions executable by a processor to form, from a single tracking pulse, in-parallel-directed receive lines for making measurements of a monochromatic shear wave.

30 [0024] Further, in some versions, performing shear wave dispersion ultrasound vibrometry (SDUV) comprises, over a plurality of locations by means of a plurality of passes over the locations, sampling in an interlaced pattern for making measurements of a monochromatic shear wave.

[0025] In a specific variant of these versions, the locations sampled in one from among the plural passes interleave with locations sampled in a next one from among said plural passes.

35 [0026] As a possible aspect, results of the sampling at a given one of the locations over multiple passes are compared to a reference A-line to determine displacement of the monochromatic shear wave at that location.

[0027] Analogously, in some aspects a device for performing shear wave dispersion ultrasound vibrometry (SDUV) is configured for, over a plurality of locations by means of a plurality of passes over the locations, sampling in an interlaced pattern for making measurements of a monochromatic shear wave.

40 [0028] What is proposed herein likewise can take the form of a method for performing shear wave dispersion ultrasound vibrometry (SDUV), which includes making measurements of a monochromatic shear wave and applying, to the measurements, a bank of filters that are tuned to respective candidate speeds of the wave, without the need to determine a difference between phases of the wave at different spatial locations.

45 [0029] In a further aspect, a low-pass filter may be used on the measurements, to reduce noise in preparation for the applying.

[0030] In yet another aspect, the filters in the bank are two-dimensional, one dimension being spatial location and the other dimension being time.

50 [0031] In an additional aspect, a device for performing shear wave dispersion ultrasound vibrometry (SDUV) is configured for making measurements of a monochromatic shear wave and applying, to the measurements, a bank of filters that are tuned to respective candidate speeds of the wave, all without the need to determine a difference between phases of the wave at different spatial locations.

[0032] As further, additional aspects, apparatus and devices described above may be implemented as one or more integrated circuits.

55 [0033] Details of the novel, fine-spatial-sampling methodology for SDUV are set forth further below, with the aid of the following drawings.

BRIEF DESCRIPTION OF THE DRAWINGS**[0034]**

5 FIG. 1 is a schematic diagram exemplary of two consecutive SDUV samples;
 FIG. 2 is a timeline of an example representative of sequential SDUV tracking;
 FIG. 3 is a flow chart corresponding to the timeline of FIG. 2;
 FIG. 4 is a schematic, transmit-receive diagram illustrating, by example, SDUV sample acquisition using retrospective
 dynamic transmit (RDT) as implemented on a 16x multiline beamformer;
 10 FIG. 5 is a schematic diagram demonstrating, in an RDT context, a possible placement of a detection beam transmit
 focus;
 FIG. 6 is a graphical rendition of an exemplary interlaced sampling scheme; and
 FIG. 7 is a flow chart representative of particular embodiments as examples of how to determine tissue shear
 elasticity and viscosity.

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DETAILED DESCRIPTION OF EMBODIMENTS

[0035] A general discussion is first had of one version of SDUV with faster sampling. What follows, in this context and
 starting with FIG. 4, is further exemplary development related to finer spatial sampling.

20 **[0036]** FIG. 1 depicts, by way of illustrative and non-limitative example, a relation between two consecutive SDUV
 samples. An ultrasound pushing probe 104 is shown, along with first and second tracking pulses 108, 112 issued at
 respective sampling times t_1 , t_2 , by an ultrasound tracking probe (not shown). The pushing probe 104 sends out a series
 of focused pushing pulses (or "pushes") 114 to establish a shear wave 115, a frequency component of which (or "mon-
 25 ochromatic shear wave") is represented by a first trace 116. Tissue vibrates along the y-direction and the shear wave
 115 propagates along the x-direction.

[0037] Two separate probes can be used for pushing and tracking respectively. However, this type of bulky configuration
 is not practical for clinical applications.

[0038] In addition, in the case of separate single-element transducers, it requires repeated firing of the push pulses
 in order to measure the shear wave phase delay at different lateral positions, resulting in repeated tissue heating.

30 **[0039]** If, on the other hand, tracking is implemented with an array transducer, the need for repeated pushes is alleviated
 in accordance with the proposal herein.

[0040] Moreover, one single array transducer can serve both functions of pushing and tracking. A dual-purpose single
 array transducer would make the system more compact and easier to control. However this configuration needs more
 hardware and software support to ensure it is feasible to generate acoustic radiation force and image the resulting shear
 35 wave 115 by a single transducer. The single transducer can be a single-row array (1D transducer) or multiple-row array
 (1.75 or 2D transducer) that allows for lateral and elevation push and/or tracking pulse locations.

[0041] Advanced 2D array technology will allow tracking pulses to be sent in 3D dimensions; however, the following
 discussion relates to tracking tissue motion in the axial-lateral plane. The same treatment applies to the axial-elevation
 plane, without loss of generality.

40 **[0042]** The tracking pulses 108, 112 are targeted to respective locations 120, 124 spatially separated by an inter-
 location distance 128 of Δr . The distance 128 is typically in the millimeter range, because the shear wave 115 attenuates
 with propagation distance. An amplitude (or displacement) 132, as represented on the y-axis 136, is measured. Based
 on the amplitude 132, a phase 140 of Φ_1 at the location 120 can be derived, provided the Nyquist threshold is met
 regarding sampling frequency. The Nyquist threshold can be met by sufficient frame rate, i.e., multiple sampling passes
 45 over the location 120 with sufficient frequency.

[0043] FIG. 2 depicts one example of sequential SDUV tracking. Before any push pulses 114 vibrate the region of
 interest (ROI), reference tracking pulses 202, 204, 206, 208 issue, targeted to respective sampling locations x_1 , x_2 , x_3 ,
 x_4 . The locations x_1 , x_2 , x_3 , x_4 are aligned radially out from a point x_0 , i.e., in a propagation direction of the shear wave
 115 to be created by the push pulses. The reference tracking pulses 202, 204, 206, 208 are each followed respectively
 50 by their echoes 210, 212, 214, 216. Then, the shear wave 115 is established at a location x_0 , i.e., the site of the excitation
 point. This is done by an initial series (not shown in FIG. 2) of push pulses 218 that are fired at a push frequency 219
 which might typically be approximately 100 Hz. A tracking-sequence-initiating onset of the push pulses 218 can issue
 once the wave 115 has been established. A pass 220 of tracking pulses 222, 224, 226, 228 follows, steered, serially,
 pulse-by-pulse. The tracking pulses 222, 224, 226, 228 are targeted to the respective sampling locations x_1 , x_2 , x_3 , x_4 .
 55 Each of the pulses 222, 224, 226, 228 is followed by its respective echo 230, 232, 234, 236, from which the respective
 receive A-line is then beamformed. The pass 220 issues at a same-location tracking frequency 238 of 2 KHz. Accordingly,
 20 passes (i.e., "frames") 220 can follow the push 218. Also, the same-location tracking frequency 238 of 2 kHz allows
 phase measurement of components 116 of frequencies of up to about 1 kHz, the Nyquist threshold. Each of the tracking

pulses 222, 224, 226, 228 can serve to simultaneously provide measurement of each of the frequency components, within the inherent limits of the Nyquist threshold.

[0044] Regular B-mode imaging is utilized, i.e., the tracking pulses 222, 224, 226, 228 are electronically focused and steered back and forth laterally at different locations x_1, x_2, x_3, x_4 between two adjacent pushing pulses 218. Receive A-lines at different locations x_1, x_2, x_3, x_4 are therefore formed sequentially.

[0045] The number of transmission lines within each B-mode frame should be limited so that the sampling PRF (pulse repetition frequency) for the shear wave 115 is high enough. As seen in FIG. 2, for example, for each location x_1, x_2, x_3, x_4 , the same-location tracking frequency 238 is 2 KHz (PRF₂), while the transmission A-line frequency 242 is 8 KHz (PRF₃). This is merely illustrative. If the highest harmonic measured is 400 Hz, this indicates that the detection pulses (laterally identically in a given direction) should be fired at a minimum rate of say 1000Hz (allowing a small margin over Nyquist). In this case, PRF₂ would be set to 1 kHz. Therefore it will be possible to transmit beams to 8 kHz/1 kHz = 8 locations.

[0046] Merely a single push/tracking sequence 240 is needed to obtain all of the SDUV information needed for shear wave speed estimation. Faster data acquisition is a key requirement to advance the technique of SDUV from a single-point "virtual biopsy" tool to a possible real-time imaging modality. Notably too, the heat generated in the tissue and transducer can be decreased while maintaining the number of lateral locations x_1, x_2, x_3, x_4 ... observed for shear wave tracking. The faster data acquisition can also further reduce noise in shear wave displacement estimation, especially therefore avoiding large temporal-scale noise such as respiratory motion that tissue might otherwise experience over the course of different push/tracking sequences 240.

[0047] FIG. 3 is a flow chart corresponding to the timeline of FIG. 2. Focus is set to the first location x_1 (step S304). A current tracking reference pulse 202 is emitted (step S308). Its echo 210 follows (step S312). If there are more locations (i.e., x_2, x_3, x_4) to be measured (step S316), the focus is steered to the next location (step S320), and processing returns to the tracking reference pulse emitting step S308 with that next location as the current location. On the other hand, if there are no further locations to be measured (step S316), the push pulse 218 is fired successively to establish the shear wave 115 (step S324). The focus is then set to the first location x_1 (step S328). The current tracking pulse 222 is emitted (step S330), and its echo 230 returns (step S332). If there are more tracking pulses (i.e., 224, 226, 228) to issue in the current pass 220 (step S333), the focus is set to the corresponding next location (step S334) and processing returns to the tracking pulse emitting step S330 with the next location as the current location. Otherwise, if there is no next tracking pulse to be emitted, query is made as to whether another pass is to be made over the locations x_1, x_2, x_3, x_4 (step S336). If a next pass is to be made, that next pass is made the current pass (step S340), and processing returns to the beginning of the next pass 220 at the step S328. If, however, there is no next pass 220 to be made (in the current push/tracking sequence 240), sampling is completed. A single push/tracking sequence 240 suffices, in the instant proposed technique, to provide all of the sampling needed for SDUV determination of shear wave speed and, in practical embodiments, for calculation of tissue elasticity and viscosity.

[0048] FIG. 4 represents one example of an SDUV sample acquisition scheme 400 using retrospective dynamic transmit (RDT), as implemented on a 16x multiline beamformer, i.e., a beamformer that forms 16 receive lines from one transmit beam (or "transmit" for short).

[0049] With a multiline beamformer, SDUV sampling will still be sequential, but by group of spatial locations. To each group, a transmission beam is issued. If the ROI is located at a different depth than the focus of the transmission beam, then the transmission beam will be broader than at the focus and will insonify the group of spatial locations. Alternatively, the beam can be weakly focused at the same depth as the ROI, with a breadth that is sufficient to insonify the group of spatial locations.

[0050] From the echoes of a transmission beam created from a single tracking pulse 404, 16x beamforming circuitry forms 16 in-parallel-directed receive lines 411-426 for making measurements of the monochromatic shear wave 116. As indicated by a diagonal, sub-aperture tracking line 427, the first eight receive lines 411-418 are on one side of the center of the transmit, and the second eight receive lines 419-426 are on the other side.

[0051] Other tracking pulses 428, 429, 430, and the first tracking pulse 404, are all differently-timed. If the transmission A-line (or "tracking pulse") PRF 242 is set equal to 10 kHz for example, the single tracking pulse 404 issues 100 μ s before the next tracking pulse 428. 100 μ s later, the next pulse 429 fires, and so on.

[0052] Each of the tracking pulses 404, 428, 429, 430 is formed by a respective then-currently active sub-aperture of the tracking probe. The active sub-aperture is a subset of the transducer elements that are currently active to transmit ultrasound. Thus, for example, after the tracking pulse 404 fires, the currently active sub-aperture shifts (e.g., one or more elements on one side of the aperture are excluded and one or more elements on the other side are included). When the next tracking pulse 428 then fires, it occurs from the shifted sub-aperture. The spatial distance between adjacent apertures is referred to hereinafter as a transmit spacing 434, which, in the current example, is 0.5 mm. The focal point of the tracking pulse also shifts by the transmit spacing 434 between consecutive tracking pulses.

[0053] The 16 in-parallel-directed receive lines 411-426 (i.e., dynamically-formed receive lines that are spatially parallel) are formed from the echo data received after the transmit 404. Each of the receive lines 411-426 is formed by a receive

sub-aperture. The receive sub-aperture is a subset of the transducer elements that contribute to a given receive line.

[0054] The spatial distance between the receive lines 411-426 is referred to hereinafter as a receive spacing 438. In this example, it is 0.125 mm, or one quarter of the 0.5 mm transmit spacing 434.

[0055] Making the receive spacing 438 a fraction of the transmit spacing 434 allows for more dense sampling, as will be discussed in more detail below.

[0056] All of the acquired echo radiofrequency data is saved in temporary storage. Retention of acquired data will continue as the sub-aperture shifts and eventually assumes its final position in the transducer array, i.e., so that an entire pass of data is acquired. In addition, data will be retained pass-to-pass.

[0057] Due to the shift in sub-aperture between the firing of the first tracking pulse 404 and the next tracking pulse 428, the last twelve receive lines 415-426 of that first pulse spatially overlap, respectively, with the first twelve receive lines of that next pulse. Likewise, due to the sub-aperture shift with each succeeding tracking pulse, the last twelve receive lines of the tracking pulse 428 overlap with the first twelve receive lines of the next tracking pulse 429, and so on.

[0058] By the time the fourth tracking pulse 430 fires, respective receive lines of all four tracking pulses 404, 428, 429, 430 overlap and can be combined to form four reconstructed A-lines 441-444.

[0059] The first reconstructed A-line 441, for example, is formed from the first receive line 423, combined with the three respective receive lines of the immediately-subsequent tracking pulses 428-430. The combining occurs in accordance with retrospective dynamic transmit (RDT). The effect of RDT focusing can be analyzed using the virtual transducer approximation proposed by Passman and Ermert in 1996. See C. Passmann & H. Ermert, "A 100-MHz ultrasound imaging system for dermatologic and ophthalmologic diagnostics," IEEE Trans. Ultrasonics, Ferroelectrics and Frequency Control, vol. 43, no. 4, pp. 545-52 (1996). This technique is further discussed in commonly-assigned U.S. Patent Publication Number 2009/0069693 to Burcher et al., entitled "Retrospective Dynamic Transmit Focusing for Spatial Compounding," (hereinafter "the '693 publication").

[0060] The first reconstructed A-line 441 is for measuring the shear wave 115 at a spatial location 451. Likewise, the immediately-subsequent reconstructed A-lines 442-444, which are laterally offset from the first reconstructed A-line 441, are for measuring the shear wave 115 at respective spatial locations 452-454.

[0061] Although here four receive lines are combinable per reconstructed A-line, fewer receive lines can be combined. The number that are actually combined depends on the depth of the ROI and its consequent insonification coverage by tracking pulse. Also, the instant example is not limitative. Thus, the aperture shift may be to an extent that more or fewer receive lines are combinable to form a reconstructed A-line.

[0062] By virtue of the combining, depth of field (DOF), the region over which the transmit is well-focused, and signal-to-noise ratio (SNR) are increased. In comparing the reconstructed A-line 441 to any of the receive A-lines from which it is reconstructed, the length over which its spatial resolution is useful has been increased by the greater DOF afforded by RDT.

[0063] A-line reconstruction based on potentially four receive lines begins with the first four reconstructed A-lines 441-444, and proceeds with each new tracking pulse. Thus, the next tracking pulse allows for the formation of four new reconstructed A-lines at respective spatial locations. Likewise, for the rest of the frame, each succeeding tracking pulse leads to the formation of a respective plurality of reconstructed A-lines, that plurality being, in the current example, made up of four reconstructed A-lines.

[0064] The shear wave 115 is therefore finely sampled, without a reduction in the pace by which tracking pulses issue.

[0065] It is noted that non-RDT embodiments are possible, where they receive focal locations are not staggered overlapping but merely adjoin one another. The shear wave 115 is still finely sampled without a reduction in the pace of tracking pulse issuance. The number of in-parallel-directed receive lines per tracking pulse may be four, for example - two on one side of the tracking beam and two on the other side.

[0066] FIG. 5 demonstrates, in an RDT context, a possible placement of a focus 504 of a detection beam 508 formed by the tracking pulse 404. A region of interest (ROI) 512, as indicated by the square outline, is where a shear wave 516 is present. In order to ensure that insonification by the detection beam 508 spans the locations to be sampled by means of the receive lines to be acquired, it would be advantageous to place the focus 504 deep to the ROI 512. A physical focus position shown in FIG. 5 is at 70 mm, a common depth 518 for transmits insonifying a given point in the ROI and therefore to be RDT-combined. Although the detection beam 508 is wide at the depth 520 of the ROI 512, the RDT reconstructed detection beam will, at that depth, be narrow - having the same width as at the (physical) focus 504. In effect and by way of example, from among the temporally-initial tracking pulse 404, and at least one laterally-offset tracking pulse 428-430 forming a transmit to be RDT-combined with that of the temporally-initial tracking pulse, at least some are focused to a common depth 518. A shallower transmit focus, to the depth 520, is reconstructed based on echo data from those of the pulses 404, 428, 429, 430 focused to the common depth 518.

[0067] This also allows the use of a larger transmit aperture 524, which may increase the total power that can be transmitted in the detection beam 508. More power affords greater sensitivity to the minute wave amplitude displacements 132, on the order of about 10 μm .

[0068] Alternatively, the focus 504 of the detection beam 508 may be placed shallow to the ROI 512.

[0069] There are additional considerations when applying RDT to SDUV.

[0070] Firstly, RDT assumes that the tissue does not move between transmit events. If displacement does occur, then it will reduce the coherence between the combined transmits and lead to signal cancellation. This would therefore appear to be incompatible with SDUV, since the tissue is being displaced by the shear wave. However, in practice the displacements 132 are of such small magnitude (typically <10 μm) that this is a small fraction of the wavelength of the tracking pulse (e.g. 300 μm at 5 MHz). Therefore, the shear wave displacements 132 will not cause any significant loss in coherence during the transmit reconstruction.

[0071] Secondly, even with non-multiline sequences 220, because the beams at different lateral locations x_1, x_2, x_3, x_4 are fired consecutively, the displacement estimates at different lateral locations are sampled at different times $t_1, t_2 \dots$

[0072] With reference back to FIG. 1, and, assuming for example a non-multiline sequence, for simplicity of demonstration, if the sampling times t_1, t_2 were simultaneous, return data, i.e., echo data, from the tracking pulse 112 would have suggested a phase 142 corresponding to sampled point 148 on the first waveform 116.

[0073] However, the sampling times t_1, t_2 are not simultaneous if tracking pulses are sequentially fired for these two locations 120, 124. (Likewise, a reconstructed A-line subsequent, in the frame, to the reconstructed A-line 444 would be a sample of the wave 115 at a different time.)

[0074] In fact, by the time t_2 , the shear wave component 116 has propagated forward, as a waveform having a frequency component represented by a second trace 144.

[0075] The corresponding sampled phase 152 of Φ_2 , on the second trace 144, differs from the phase 140 of Φ_1 , on the first trace 116, by a phase difference of $\Delta\Phi = \Phi_2 - \Phi_1$.

[0076] As seen from FIG. 1, $\Delta\Phi$ is less than the difference between the phases 140, 142 that simultaneous tracking pulses would have fetched.

[0077] As further seen from FIG. 1, $\Delta\Phi$ is smaller by an intersample-delay-based phase correction 156 of $\omega\Delta t$, " ω " representing the angular frequency of the monochromatic shear wave 116, with " Δt " signifying the delay between the taking, at the respective sampling times t_1, t_2 , of the two samples.

[0078] Yet it is the difference between the phases 140, 142 that, along with ω and Δr , define the propagation speed of the shear wave frequency component 116.

[0079] That difference is calculated by adding, to the phase difference $\Delta\Phi$, the intersample-delay-based phase correction 156 of $\omega\Delta t$.

[0080] The speed of the monochromatic shear wave 116 is given by the following formula:

$$c_s(\omega) = \frac{\omega\Delta r}{\Delta\phi + \omega\Delta t} \quad \text{(formula 1)}$$

[0081] A derivation of the formula 1 is as follows:

$c_s(\omega) = \lambda f$, where c_s is propagation speed, λ is the wavelength, " ω " represents the angular frequency of the monochromatic shear wave 116 and f is the wave's frequency.

[0082] Also, $\omega = 2\pi f$, and $\Delta r = \lambda\Delta\Phi/2\pi$, where $\Delta\Phi$ represents the phase difference, for a given moment, between the two samples taken simultaneously.

[0083] All parameters are assumed to be positive.

$$c_s(\omega) = \frac{\omega\Delta r}{\Delta\phi}$$

[0084] Substituting values yields

[0085] To account for the intersample delay between the two differently-timed samples taken at the times t_1, t_2 , the intersample-delay-based phase correction 156 of $\omega\Delta t$ is added to $\Delta\Phi$ to arrive at formula (1), as explained above in connection with FIG. 1.

[0086] The same phenomenon occurs with an RDT sequence, and must be taken into account when extracting amplitude information based on A-lines directed differently and acquired at different times, e.g., the reconstructed A-line 444 and a reconstructed A-line later acquired in the frame.

[0087] To account for this in the application of formula 1, when RDT combines transmits to interpolate intermediate transmit locations (as disclosed in the '693 publication), the sampling time (as well as the sampling location) is interpolated between transmits. In other words, in the case of pulse firing times, and in the case of the transmit locations upon firing (e.g., those along the sub-aperture tracking line 427 for transmits used in the reconstruction), they are interpolated by the same RDT interpolation weightings. Thus, Δt and Δr can be computed for substitution into formula (1).

[0088] It is noted that formula (1) assumes tracking, i.e., the emission of tracking pulses, in the (radial) outward direction of shear wave propagation. If tracking is performed in the reverse direction, the "+" sign in the denominator becomes a "-" sign. By analogous reasoning, if the tracking direction alternates with passes 220, the $\Delta\Phi$ calculation for a pair of spatial locations 120, 124 can be averaged with the same calculation made based on an adjoining pass, so that the

denominator is simply $\Delta\Phi_{\text{avg}}$.

[0089] Formula (1) also assumes the two differently-located samples were acquired at different times.

[0090] In the non-RDT, non-multiline example illustrated in FIGs. 2 and 3, differently-located samples are acquired at different times.

[0091] In a non-RDT, multiline embodiment, the receive lines of a given transmit are not differently timed. So, the intersample-delay-based phase correction 156 of $\omega\Delta t$ is omitted from the denominator of formula (1) for those speed calculations, if any, based on receive lines of a given transmit. However, formula (1) is otherwise used, as is.

[0092] In an RDT context, a reconstructed A-line subsequent, in the frame, to the reconstructed A-line 444 would be a sample of the wave 115 at a different time. Likewise, the reconstructed A-lines 441-444 will generally have different sampling times, the latter being based on the respective interpolations of transmit firing times. Those respective interpolations each use different interpolation weights which are proportional to the transmit field strength at the target location along the A-line to be reconstructed. Typically, then, the first reconstructed A-line 441 will have an earlier sampling time than the immediately-subsequent reconstructed A-line 442 for purposes of the speed calculation. So, formula (1) is applicable as is.

[0093] FIG. 6 exemplifies an interlaced sampling scheme 600. It does not rely on a multiline beamformer or RDT. For simplicity it will therefore be described for a basic beamformer capable of forming only a single receive line per tracking pulse 222. The x-axis 604 is lateral position, in millimeters, from the first sampling location x_1 . The y-axis 608 is the time transpired since the first tracking pulse 222. A motion field 612 of measured displacements 616, whose magnitudes are not shown, is represented. The observations 616 are indicated for several sampling passes over the sampling locations $x_1, x_2, x_3, x_4 \dots$

[0094] The present inventors have observed that it would be desirable to create a sample scheme in which samples that ordinally match an appropriately-spaced-apart pattern, (e.g., 1st, 4th, 7th, 10th ...), "ride" the propagation wave phase-wise in-place, or approximately so. Each of the respective displacements 616 would, accordingly, be nearly the same, thereby reducing sampling artefacts. Such a device is particularly beneficial when faced with tight PRF and other implementation constraints.

[0095] As previously noted, the rate of temporal sampling is limited by the maximum frequency of the shear waves. To sample a 400 Hz shear wave well requires a temporal sampling rate of at least 1000 Hz. In turn, the total sampling rate (over all locations) is bound by the maximum PRF 242 permitted by the imaging depth. The maximum PRF 242 may be, as mentioned above in connection with an example, 10 kHz, which dictates that at most 10 spatial locations can be sampled without risking the emergence of sampling artefacts such as aliasing.

[0096] To summarize, it is desirable to sample many lateral locations x_1, x_2, x_3, x_4 to increase the number of measurements for robustness. The number of lateral positions is limited by the maximum PRF 242 as noted just above, although the PRF should be large enough to allow for enough locations to be sampled without sampling artefacts.

[0097] It is also of benefit that the lateral locations be as close to the excitation point x_0 as possible to avoid attenuation of the shear wave amplitude which makes it hard to measure the amplitude, although the first lateral location x_1 is limited in its closeness to the excitation point, due to near-field effects. The closeness between locations x_i, x_{i+1} is constrained, however, by other engineering considerations.

[0098] The interlaced sampling scheme 600, in which sampling in one pass is location-wise interleaved with sampling in the next pass, takes advantage, firstly, of the fact that the motion field to be measured is highly structured: it consists of shear waves 116 with a limited range of speeds.

[0099] Secondly, the nature of the two axes 604, 608, relating to position and time, respectively, is such that sampling consecutive locations $x_i, x_{i+1}, x_{i+2} \dots$ implies a constant tracking-pulse translation speed. This is seen in FIG. 6 from the first row 620 of observations. Since they imply a line of constant slope, a constant tracking-pulse translation speed is implicit. In this context and with regard to the constant tracking-pulse "translation," if the beam is steered in a non-parallel manner, the "translation" can be considered to occur between lateral locations x_i, x_{i+1} .

[0100] However, the above design criteria call for a higher translation speed than any of the monochromatic wave speeds c_s .

[0101] A slower, constant tracking-pulse translation speed is, nevertheless, discernible by confining scrutiny to the sampling of two consecutive locations x_i, x_{i+1} by means of separate passes 220. This is exemplified by the slanted line 624, characterized in that samples of interest at the two locations x_i, x_{i+1} are in consecutive passes 220.

[0102] The same phenomenon of higher- and slower-speed patterns exists for a non-interlaced motion field, i.e., a field in which in each pass 220 consecutive locations x_i, x_{i+1} are sampled without skipping locations

[0103] However, interlacing the sampling is a tool by which to craft more different constant tracking-pulse translation speeds, thereby increasing the potential to achieve a match (or near match as seen from the line 624) with the speed of the targeted shear wave 116. The need for such a technique arises because of the difficulty in otherwise manipulating parameters to alter the translation speed, given the above-discussed design constraints. Notably, too, interlacing the sampling results in the same number of samples. Also, it does not adversely impact the tracking pulse PRF 242, which remains constant.

[0104] As seen from FIG. 6, the motion field 612 is segmentable into observation lines parallel to the central, slanted line 624.

[0105] The consequent reduction of sampling artefacts can serve to mitigate any potential side effects of finer spatial sampling.

5 [0106] FIG. 7 shows particular embodiments as examples of how to determine tissue shear elasticity and viscosity. A first component 116, e.g., the fundamental, of a shear wave 115 is selected as the current component (step S704).

[0107] Echo RF data, which, in the RDT context, consists of the temporally-initial reconstructed A-lines 441-444, the ones subsequent in the frame, and ones in other frames, are acquired, in accordance with the multiline sample acquisition scheme 400 for example (step S708). For each of the spatial locations 451-454 ..., the reconstructed A-lines at that location are each compared to the corresponding reconstructed reference A-line to determine the displacement 132 of the current wave component 116 at that location. A number of known approaches, such as cross-correlation or Doppler approaches can be used to calculate the displacements 132.

[0108] Likewise, in non-RDT, multiline and non-multiline contexts, same-located samples are compared (step S712).

15 [0109] Because of the finer sampling in accordance with the methods proposed herein, application is made, optionally, in some embodiments, of a low-pass filter (LPF) to the measurements 132 to reduce noise in the measurements. The LPF can be a two-dimensional filter for acting in the location and time dimensions 604, 608. An example of such a filter would be an anisotropic filter, such as a Gaussian kernel:

$$20 \quad kg = \exp(-(r^2/\sigma_1^2 + t^2/\sigma_2^2)), \quad \text{formula (2)}$$

where "r" represents location, "t" represents time, and σ_1 and σ_2 control the size of the filter in the spatial and temporal dimensions respectively.

25 [0110] If the motion field 612 consists of a single shear wave 116, then a contour on the motion field with constant displacement (i.e., since the interlaced scheme 600 is arranged, by appropriate intersample spacings on the axes 604, 608, to result in the slanted line 624 of essentially constant displacements 616) is a straight line which slopes, down and to the right, and whose slope or "gradient" is determined by the speed of the shear wave 116.

[0111] The motion field 612 can be represented by a two-dimensional matrix of displacements 616, one dimension being location and the other being time. Similarly, the expression on the right side of formula (1) is evaluated to create another two-dimensional matrix, the two matrices being convolved to reduce noise in the measurements 616.

30 [0112] An alternative filter is a steered filter:

$$35 \quad ks = \exp(-(u^2/\sigma_3^2 + v^2/\sigma_4^2)), \quad \text{formula(3)}$$

$$u = r + cs \times t$$

$$v = r - cs \times t$$

40 where cs is the angle of the filter (which represents a speed), "u" is in a direction aligned with the contours of waves propagating forward with a speed cs, and "v" is in a reverse direction aligned with the contours of hypothetical waves that could be imagined to be propagating backward, i.e., toward the excitation point x_0 , with a speed cs. Sizing parameters σ_3, σ_4 control the size of the filter in the two directions, u and v. Typically, σ_3 will be larger than σ_4 , so that more smoothing is applied in the v direction than the u direction.

[0113] If the motion field 612 consists of a single shear wave 116 propagating forward with speed cs, then lines of constant v will lie along contours on the motion field with constant displacement. The filter kernel ks in formula (3) will be aligned with the motion field 612. The angle of the filter is, in this context, given by the *a priori* speed of the shear wave 116. Optionally, the filter angle can be adjusted iteratively using the current estimate of the shear wave speed.

[0114] Convolution of the kernel ks with the measurements 132 will smooth more in the parallel direction to the contour than in the perpendicular direction. Therefore for a given amount of noise reduction, it will tend to preserve the structure of the motion field 612 better than an isotropic filter (step S716).

50 [0115] An alternative to determining a difference between phases of the shear wave 116 at different spatial locations x_i, x_j , as in accordance with formula (1), is to apply a bank of two-dimensional filters, each tuned to a specific candidate wave speed.

[0116] If the filter bank is to be applied (step S720), a number of filters are used, covering the expected range of wave speeds. The motion field 612 is convolved with each of the filters (in turn, or in parallel). The filter with the largest output is taken as the best estimate of wave speed. The process can be iterated, making the estimate more accurate by tuning the filters to a more closely spaced selection of wave speeds, around the current estimate.

[0117] As an example, a motion field is represented in the form:

$$d(r,t) = d(n\Delta r, m\Delta t) \quad \text{formula (4)}$$

where "r" is the lateral position, "t" is the acquisition time, and "n" and "m" are sample indices, Δr is the lateral sampling interval and Δt is the time between displacement samples at the same lateral position.

[0118] The motion field in this example features, for simplicity of demonstration, a regular, evenly-spaced grid, in which initial values of "t" (like "r") are implicitly initially zero. This, then, corresponds to sampling in a non-interlaced pattern, rather than in the interlaced sampling scheme 600. However, this example can be adapted to the interlaced sampling scheme by appropriately modifying formula (4) above, and formulas (5) and (6) below.

[0119] Continuing with the example, a filter which corresponds to a wave speed of c_{si} has an in-phase kernel:

$$ki(c_{si}, r, t) = \sin(2\pi / \lambda_s * (n\Delta r - c_{si} * m\Delta t)); \quad \text{formula (5)}$$

and a quadrature kernel:

$$kq(c_{si}, r, t) = \cos(2\pi / \lambda_s * (n\Delta r - c_{si} * m\Delta t)) \quad \text{formula (6)}$$

Here λ_s is the wavelength of the shear wave 116.

The output of the filter is given by

$$y(c_{si}) = (\sum_{r,t} d(r,t) \times ki(c_{si}, r, t))^2 + (\sum_{r,t} d(r,t) \times kq(c_{si}, r, t))^2 \quad \text{formula (7)}$$

[0120] An *a priori* estimate of c_{si} is used in formulas (5) and (6) to derive the kernels of a first filter. The kernels are then applied to formula (7) to yield a first output. Other filters in the bank are generated by varying the value of c_{si} in formulas (5) and (6), and recalculating $y(c_{si})$ in formula (7). The speed of the shear wave 116 is given by the value of c_{si} for which $y(c_{si})$ has the maximum value.

[0121] Improved results may be obtained by windowing the kernel. This mitigates the bias caused by the truncation resulting from the finite extent of the kernels and sampled data (step S724).

[0122] With reference again to step S720, if, instead of the filter bank, a phase-difference-based wave speed calculation is to be made, input parameters to the calculation are derived. Specifically, the phases Φ are determined for the displacements 132. This can be done by Nyquist reconstruction based on the displacements 132 observed at a given spatial location 451, 452, 453, 454..., and is performed for each of the different spatial locations. Phase differences $\Delta\Phi = \Phi_2 - \Phi_1$ are calculated pair-wise to estimate the phase difference $\Delta\Phi$ to be substituted into formula (1). These phase difference calculations are performed for respective samples acquired at different times, as, for example, in the case of the temporally-first reconstructed A-line 444 and any subsequent one in the frame. The calculated phase differences $\Delta\Phi$ for differently-timed samples are corrected respectively using the intersample-delay-based phase correction 156 of $\omega\Delta t$. At least some of the pairs selected may be relatively far apart spatially, to improve accuracy of the calculations. Least-squares analysis can be used on the phase differences (corrected or uncorrected, as the case may be) and their respective inter-location distances 128 of Δr . Formula (1) (with or without the correction 156, as the case may be) is then applied to estimate the speed of the current wave component 116 (step S728).

[0123] With either path (i.e., through step S724 or S728), if the current wave component is not the last one to be subject to speed determination (step S732), the next component is made the current component (step S736).

[0124] If the same RF data used in wave speed determination for the previous component can be used for the current component, because, for example, the tracking pulse PRF 242 was sufficient for the highest harmonic (step S740), processing returns to step S712. Otherwise, if a further acquisition is to be made for the current component, processing returns, instead, to step S708.

[0125] In step S732, if the current wave component is, instead, the last one to be subject to speed determination, the Voigt model, which is well-known in the art, is applied to determine sheer elasticity and viscosity (step S744).

[0126] Shear wave dispersion ultrasound vibrometry (SDUV) is implemented in some embodiments to form, from a single tracking pulse, in-parallel-directed receive lines for making measurements of a monochromatic shear wave. In some embodiments, sampling is performed, over spatial locations by means of passes over the locations, in an interlaced pattern for making measurements of the wave. In some embodiments, measurements are made of the wave and to the measurements are applied a bank of filters that are tuned to respective candidate wave speeds, all without the need to determine a difference between wave phases at different spatial locations.

[0127] By extracting more information from each tracking pulse fired, methodology and apparatus as proposed herein

afford a more complete sampling of the shear wave displacement field. This therefore allows for more robust estimation of the shear wave speed and the elastic properties of the medium.

[0128] The methods proposed herein can be implemented in software or, for example, in an article of manufacture inclusive of a device, which can be realized as one or more integrated circuits.

[0129] An embodiment employing RDT may be realized, for instance, as a single beamformer, such as a 16x or 32x multiline beamformer, hardware being added just for buffering, and the combining of overlapped receive lines.

[0130] It should be noted that the above-mentioned embodiments illustrate rather than limit the invention. For example, the methods disclosed herein may be implemented in any of various scanning geometries (linear, phased or curved). In the claims, any reference signs placed between parentheses shall not be construed as limiting the claim. Use of the verb "to comprise" and its conjugations does not exclude the presence of elements or steps other than those stated in a claim. The article "a" or "an" preceding an element does not exclude the presence of a plurality of such elements. The invention may be implemented by means of hardware comprising several distinct elements, and by means of a suitably programmed computer having a computer readable medium. The mere fact that certain measures are recited in mutually different dependent claims does not indicate that a combination of these measures cannot be used to advantage.

Claims

1. A method for performing shear wave dispersion ultrasound vibrometry (SDUV), comprising:

establishing a shear wave having a monochromatic shear wave component; and
 initiating a sequence of consecutive tracking pulses (404) to sequentially sample a group of spatial locations (451,452,453,454), wherein each of the tracking pulses is formed from a sub-aperture of a tracking probe and it insonifies the group of said spatial locations, wherein the sub-aperture used to form consecutive tracking pulses shifts by a so called transmit spacing and the focal point of each of the consecutive tracking pulses also shifts by the transmit spacing,
 forming from the echoes received after transmission of each tracking pulse with a multiline beamformer by means of retrospective dynamic transmit (RDT), a plurality of in-parallel-directed receive lines (411-426) for making measurements of the monochromatic shear wave component (116), wherein the in-parallel-directed receive lines are dynamically-formed receive lines that are spatially parallel,
 and wherein each of the in-parallel-directed receive lines is formed by another receive sub-aperture of the tracking probe.

2. The method of claim 1, wherein said forming a plurality of in-parallel-directed receive lines from at least one tracking pulse, is executed so as to overlap resulting receive lines (423-426) to increase a measurement depth of field.

3. The method of claim 2, wherein increasing the measurement depth of field entails combining from among the overlapped ones of in-parallel-directed receive lines to create at least one reconstructed A-line (441-444).

4. The method of claim 3, wherein one other tracking pulses includes differently-timed tracking pulses, further comprising:
 forming, from the differently-timed ones (428-430) of said at least one other tracking pulse, respective pluralities of reconstructed A-lines created by said combining.

5. The method of claim 1, wherein making measurements comprise making amplitude (132) measurements of said monochromatic shear wave component.

6. An apparatus for performing shear wave dispersion ultrasound vibrometry (SDUV), comprising:

means for establishing a shear wave having a monochromatic shear wave component;
 a tracking probe for initiating a sequence of consecutive tracking pulses (404) to sequentially sample a group of spatial locations (451,452,453,454), wherein each of the tracking pulses is formed from a sub-aperture of the tracking probe and it insonifies the group of said spatial locations, wherein the sub-aperture used to form consecutive tracking pulses shifts by a so called transmit spacing and the focal point of each of the consecutive tracking pulses also shifts by the transmit spacing, and wherein the tracking probe is configured to form from the echoes received after transmission of each tracking pulse with a multiline beamformer by means of retrospective dynamic transmit (RDT) a plurality of in-parallel-directed receive lines (411-426) for making measurements of the monochromatic shear wave component (116), wherein the in-parallel-directed receive lines are

dynamically-formed receive lines that are spatially parallel,
and wherein each of the in-parallel-directed receive lines is formed by another receive sub-aperture of the tracking probe.

- 5 7. The apparatus of claim 6, wherein a single tracking pulse, and at least one other laterally-offset tracking pulse, are focused to a common depth (504), said apparatus further comprising:
means for, based on echo data from respective tracking pulses focused to said common depth, reconstructing a transmit focus at a shallower depth than said common depth.
- 10 8. The apparatus of claim 6, wherein the tracking probe is further configured to execute the forming a plurality of in-parallel-directed receive lines from at least one tracking pulse, so as to overlap a corresponding resulting plurality of in-parallel-directed receive lines, and to interpolate pulse firing times of tracking pulses to correct for intersample wave propagation (156) in determining a corresponding phase difference of the monochromatic shear wave component, measured at differently-timed sampled spatial locations.
- 15 9. The apparatus of claim 6, wherein the apparatus is implemented as one or more integrated circuits.
- 20 10. A non-transitory computer readable medium embodying a computer program that includes instructions executable by a processor for performing the shear wave dispersion ultrasound vibrometry (SDUV) method of claim 1.

Patentansprüche

- 25 1. Verfahren zum Durchführen von Scherwellendispersionsultraschallvibrometrie (SDUV), umfassend:
Aufbauen einer Scherwelle mit einer monochromatischen Scherwellenkomponente; und
Einleiten einer Sequenz von aufeinanderfolgenden Verfolgungsimpulsen (404), um eine Gruppe von räumlichen Orten (451,452,453,454) sequentiell abzutasten, wobei jeder der Verfolgungsimpulse aus einer Subapertur einer Verfolgungssonde gebildet wird und er die Gruppe der genannten räumlichen Orte beschallt, wobei sich die Subapertur, die dazu verwendet wird, aufeinanderfolgende Verfolgungsimpulse zu bilden, um einen so genannten Sendeabstand verschiebt, und der Fokus von jedem der aufeinanderfolgenden Verfolgungsimpulse sich ebenfalls um den Sendeabstand verschiebt,
30 Bilden, anhand der nach dem Aussenden von jedem der Verfolgungsimpulse empfangenen Echos, einer Vielzahl von parallel gerichteten Empfangslinien (411-426) mit einem Mehrlinien-Strahlformer mittels RDT (retrospektiver dynamischer Aussendung), um Messungen der monochromatischen Scherwellenkomponente (116) durchzuführen, wobei die parallel gerichteten Empfangslinien dynamisch geformte Empfangslinien sind, die räumlich parallel sind,
35 und wobei jede der parallel gerichteten Empfangslinien durch eine andere Empfangs-Subapertur der Verfolgungssonde gebildet wird.
- 40 2. Verfahren nach Anspruch 1, wobei das genannte Bilden einer Vielzahl von parallel gerichteten Empfangslinien anhand von mindestens einem Verfolgungsimpuls durchgeführt wird, um so resultierende Empfangslinien (423-426) zu überlappen und dadurch eine Messtiefenschärfe zu erhöhen.
- 45 3. Verfahren nach Anspruch 2, wobei das Erhöhen der Messtiefenschärfe das Kombinieren von überlappten der parallel gerichteten Empfangslinien erfordert, um mindestens eine rekonstruierte A-Linie (441-444) zu erzeugen.
- 50 4. Verfahren nach Anspruch 3, wobei ein weiterer Verfolgungsimpuls unterschiedlich zeitgesteuerte Verfolgungsimpulse einschließt, ferner umfassend:
Bilden, anhand der unterschiedlich zeitgesteuerten (428-430) des genannten mindestens einen weiteren Verfolgungsimpulses, von jeweiligen Vielzahlen von rekonstruierten A-Linien, die durch das genannte Kombinieren erzeugt werden.
- 55 5. Verfahren nach Anspruch 1, wobei das Durchführen von Messungen das Durchführen von Amplitudenmessungen (132) der genannten monochromatischen Scherwellenkomponente umfasst.
6. Gerät zum Durchführen von Scherwellendispersionsultraschallvibrometrie (SDUV), umfassend:

Mittel zum Aufbauen einer Scherwelle mit einer monochromatischen Scherwellenkomponente; Verfolgungssonde zum Einleiten einer Sequenz von aufeinanderfolgenden Verfolgungsimpulsen (404), um eine Gruppe von räumlichen Orten (451,452,453,454) sequentiell abzutasten, wobei jeder der Verfolgungsimpulse aus einer Subapertur der Verfolgungssonde gebildet wird und er die Gruppe der genannten räumlichen Orte beschallt, wobei sich die Subapertur, die dazu verwendet wird, aufeinanderfolgende Verfolgungsimpulse zu bilden, um einen so genannten Sendeabstand verschiebt, und der Fokus von jedem der aufeinanderfolgenden Verfolgungsimpulse sich ebenfalls um den Sendeabstand verschiebt, und wobei die Verfolgungssonde konfiguriert ist, um anhand der nach dem Aussenden von jedem der Verfolgungsimpulse empfangenen Echos mit einem Mehrlinien-Strahlformer mittels RDT (retrospektiver dynamischer Aussendung) eine Vielzahl von parallel gerichteten Empfangslinien (411-426) zu bilden, um Messungen der monochromatischen Scherwellenkomponente (116) durchzuführen, wobei die parallel gerichteten Empfangslinien dynamisch geformte Empfangslinien sind, die räumlich parallel sind, und wobei jede der parallel gerichteten Empfangslinien durch eine andere Empfangs-Subapertur der Verfolgungssonde gebildet wird.

7. Gerät nach Anspruch 6, wobei ein einzelner Verfolgungsimpuls, und mindestens ein weiterer seitlich versetzter Verfolgungsimpuls, auf eine gemeinsame Tiefe (504) fokussiert sind, wobei das Gerät ferner umfasst: Mittel, um basierend auf Echodaten von jeweiligen auf die genannte gemeinsame Tiefe fokussierten Verfolgungsimpulsen, einen Sendefokus bei einer flacheren Tiefe als der genannten gemeinsamen Tiefe zu rekonstruieren.
8. Gerät nach Anspruch 6, wobei die Verfolgungssonde ferner konfiguriert ist, um das Bilden einer Vielzahl von parallel gerichteten Empfangslinien anhand von mindestens einem Verfolgungsimpuls durchzuführen, um so eine entsprechende resultierende Vielzahl von parallel gerichteten Empfangslinien zu überlappen, und um Impulsabfeuerungszeiten von Verfolgungsimpulsen zu interpolieren, um bei der Bestimmung einer entsprechenden Phasendifferenz der monochromatischen Scherwellenkomponente, die an mit unterschiedlicher Zeitsteuerung abgetasteten räumlichen Orten gemessen wird, eine Korrektur in Bezug auf die Wellenausbreitung (156) zwischen den Abtastungen vorzunehmen.
9. Gerät nach Anspruch 6, wobei das Gerät als eine oder mehrere integrierte Schaltungen ausgeführt ist.
10. Nicht-flüchtiges computerlesbares Medium, das ein Computerprogramm verkörpert, welches durch einen Prozessor ausführbare Anweisungen zum Durchführen des Scherwellendispersionsultraschallvibrometrie-Verfahrens (SDUV) nach Anspruch 1 umfasst.

Revendications

1. Procédé pour réaliser une vibrométrie ultrasonore à dispersion d'onde de cisaillement (SDUV), comprenant :
 - l'établissement d'une onde de cisaillement possédant une composante d'onde de cisaillement monochromatique ; et
 - l'initiation d'une séquence d'impulsions de poursuite consécutives (404) pour séquentiellement échantillonner un groupe de localisations spatiales (451, 452, 453, 454), dans lequel chacune des impulsions de poursuite est formée à partir d'une sous-ouverture d'une sonde de poursuite et elle insonifie le groupe desdites localisations spatiales, dans lequel la sous-ouverture utilisée pour former des impulsions de poursuite consécutives se déplace selon un espacement dit de transmission et le point focal de chacune des impulsions de poursuite consécutives se déplace également selon l'espacement de transmission,
 - la formation, à partir des échos reçus après la transmission de chaque impulsion de poursuite, avec un formeur de faisceau multiligne, au moyen de transmission dynamique rétrospective (RDT), d'une pluralité de lignes de réception dirigées en parallèle (411 à 426) pour réaliser des mesures de la composante d'onde de cisaillement monochromatique (116), dans lequel les lignes de réception dirigées en parallèle sont des lignes de réception formées dynamiquement qui sont spatialement parallèles,
 - et dans lequel chacune des lignes de réception dirigées en parallèle est formée par une autre sous-ouverture de réception de la sonde de poursuite.
2. Procédé selon la revendication 1, dans lequel ladite formation d'une pluralité de lignes de réception dirigées en parallèle à partir d'au moins une impulsion de poursuite est exécutée afin de faire chevaucher des lignes de réception résultantes (423 à 426) pour augmenter une profondeur de champ de mesure.

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3. Procédé selon la revendication 2, dans lequel l'augmentation de la profondeur de champ de mesure implique la combinaison, parmi les lignes en chevauchement, de lignes de réception dirigées en parallèle pour créer au moins une ligne A reconstruite (441 à 444).
- 5 4. Procédé selon la revendication 3, dans lequel une autre impulsion de poursuite inclut des impulsions de poursuite de temps différents, comprenant en outre :
la formation, à partir des impulsions de temps différents (428 à 430) de ladite au moins une autre impulsion de poursuite, des pluralités respectives de lignes A reconstruites créées par ladite combinaison.
- 10 5. Procédé selon la revendication 1, dans lequel la réalisation de mesures comprend la réalisation de mesures d'amplitude (132) de ladite composante d'onde de cisaillement monochromatique.
6. Appareil pour réaliser une vibrométrie ultrasonore à dispersion d'onde de cisaillement (SDUV), comprenant :
- 15 des moyens pour établir une onde de cisaillement possédant une composante d'onde de cisaillement monochromatique ;
une sonde de poursuite pour initier une séquence d'impulsions de poursuite consécutives (404) pour séquentiellement échantillonner un groupe de localisations spatiales (451, 452, 453, 454), dans lequel chacune des impulsions de poursuite est formée à partir d'une sous-ouverture de la sonde de poursuite et elle insonifie le
20 groupe desdites localisations spatiales, dans lequel la sous-ouverture utilisée pour former des impulsions de poursuite consécutives se déplace selon un espacement dit de transmission et le point focal de chacune des impulsions de poursuite consécutives également se déplace selon l'espacement de transmission, et dans lequel la sonde de poursuite est configurée pour former, à partir des échos reçus après la transmission de chaque
25 impulsion de poursuite, avec un formeur de faisceau multiligne, au moyen de transmission dynamique rétrospective (RDT), une pluralité de lignes de réception dirigées en parallèle (411 à 426) pour réaliser des mesures de la composante d'onde de cisaillement monochromatique (116), dans lequel les lignes de réception dirigées en parallèle sont des lignes de réception formées dynamiquement qui sont spatialement parallèles,
et dans lequel chacune des lignes de réception dirigées en parallèle est formée par une autre sous-ouverture de réception de la sonde de poursuite.
- 30 7. Appareil selon la revendication 6, dans lequel une impulsion de poursuite unique, et au moins une autre impulsion de poursuite latéralement décalée, sont focalisées vers une profondeur commune (504), ledit appareil comprenant en outre :
des moyens pour, sur la base de données d'écho à partir d'impulsions de poursuite respective focalisées vers ladite
35 profondeur commune, reconstruire un foyer de transmission à une profondeur moins importante que ladite profondeur commune.
8. Appareil selon la revendication 6, dans lequel la sonde de poursuite est en outre configurée pour exécuter la formation d'une pluralité de lignes de réception dirigées en parallèle à partir d'au moins une impulsion de poursuite, afin de
40 faire chevaucher une pluralité résultante correspondante de lignes de réception dirigées en parallèle, et pour interpoler des temps de déclenchement d'impulsion d'impulsions de poursuite pour corriger une propagation d'onde inter-échantillon (156) dans la détermination d'une différence de phase correspondante de la composante d'onde de cisaillement monochromatique, mesurée à des localisations spatiales échantillonnées de temps différents.
- 45 9. Appareil selon la revendication 6, dans lequel l'appareil est mis en oeuvre sous forme d'un ou de plusieurs circuits intégrés.
10. Support non transitoire lisible par ordinateur incorporant un programme d'ordinateur qui inclut des instructions exécutables par un processeur pour réaliser le procédé de vibrométrie ultrasonore à dispersion d'onde de cisaillement
50 (SDUV) selon la revendication 1.
- 55

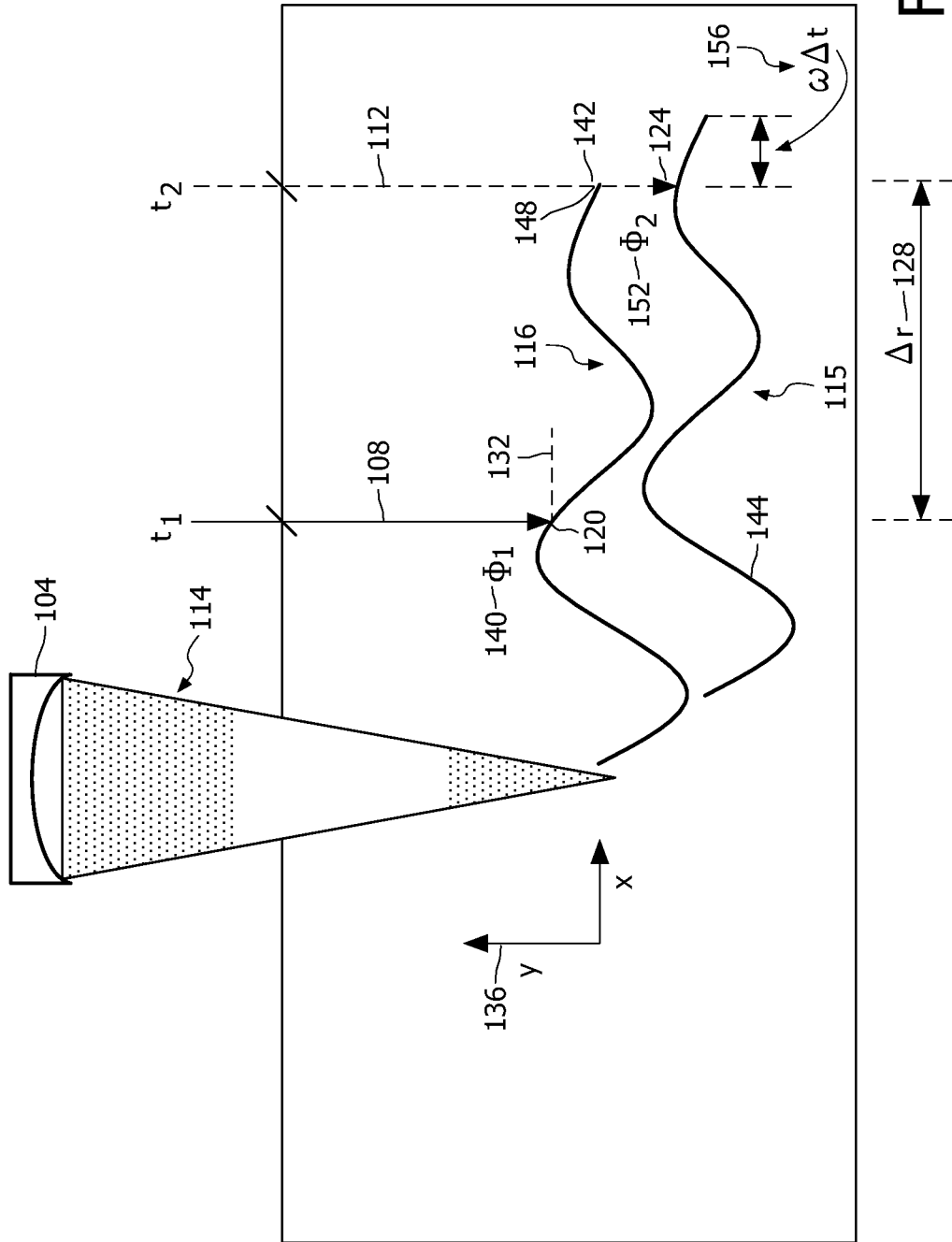


FIG. 1

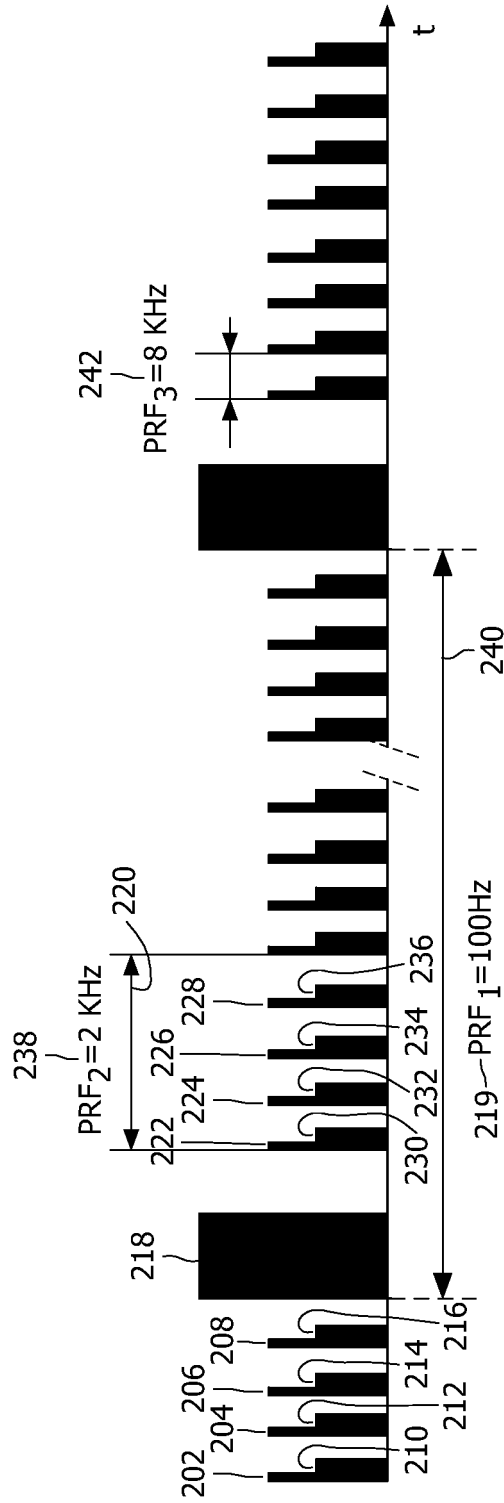


FIG. 2

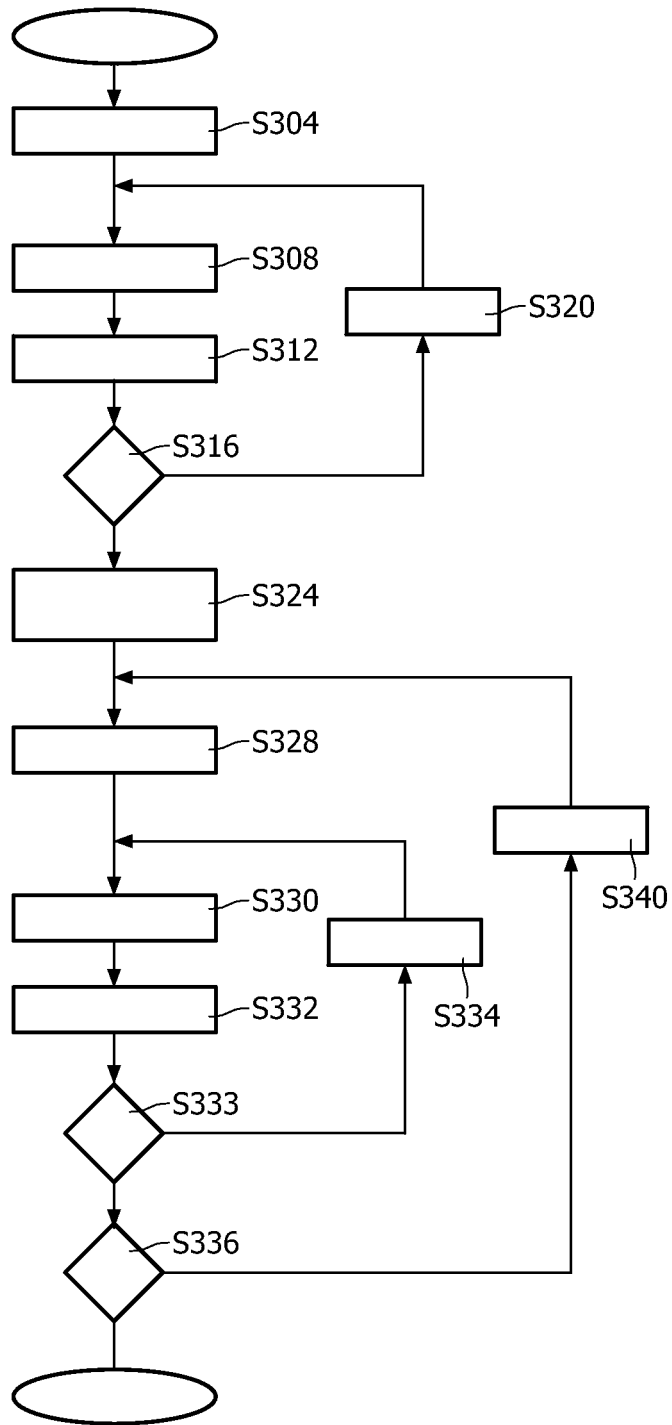


FIG. 3

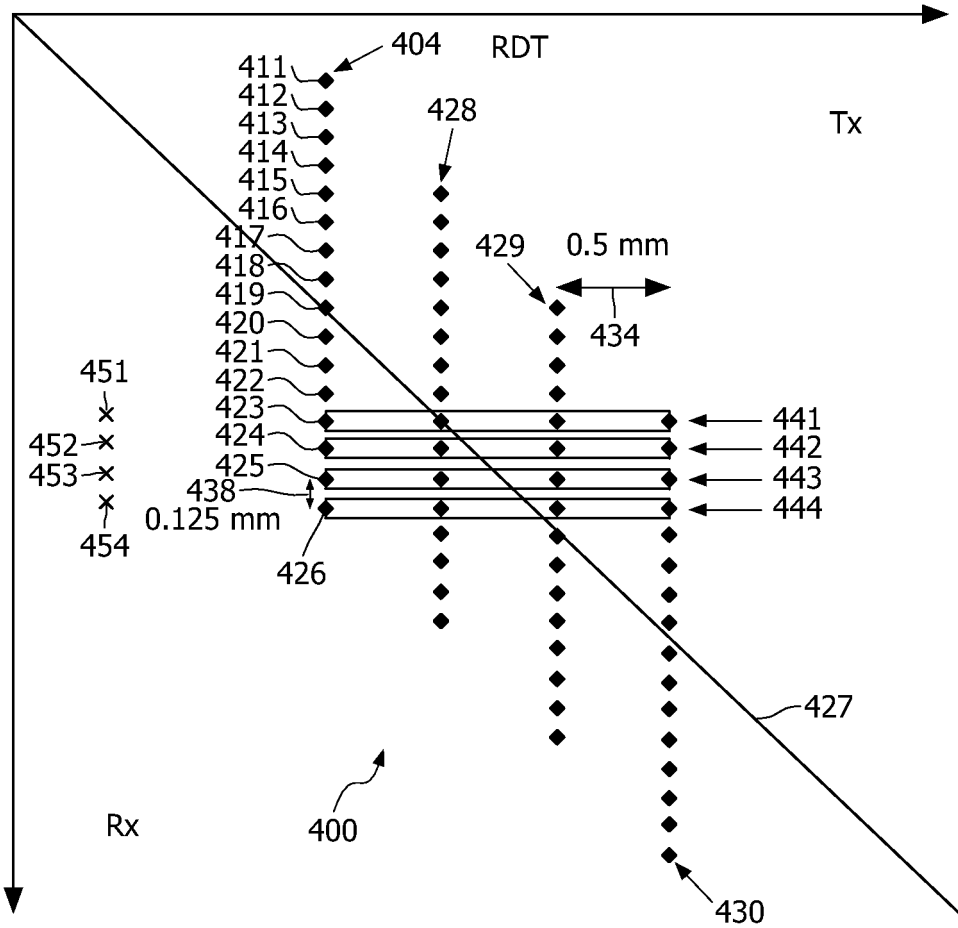


FIG. 4

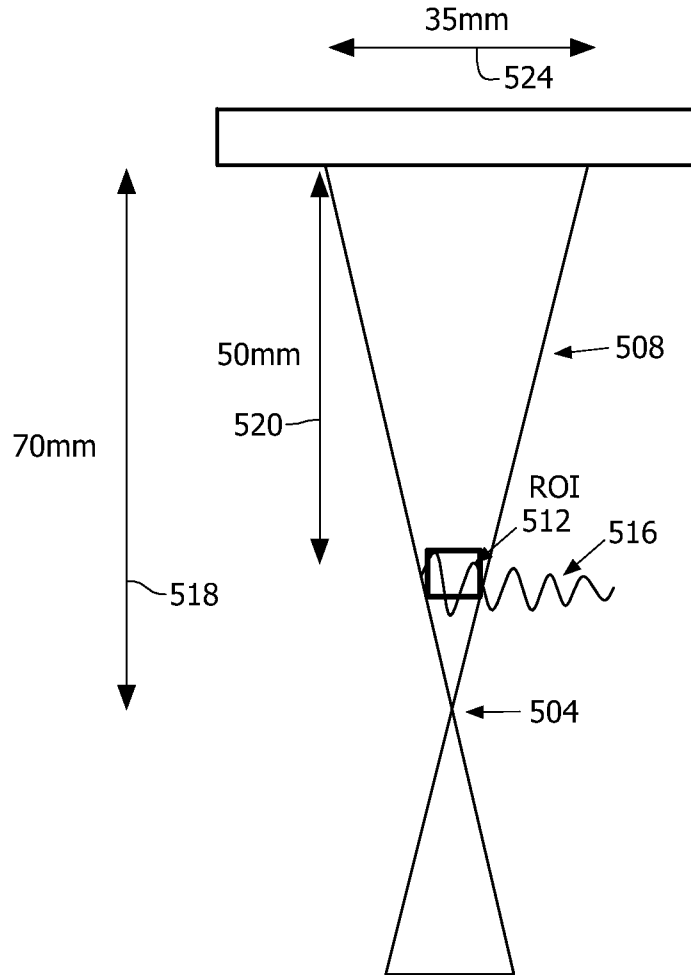


FIG. 5

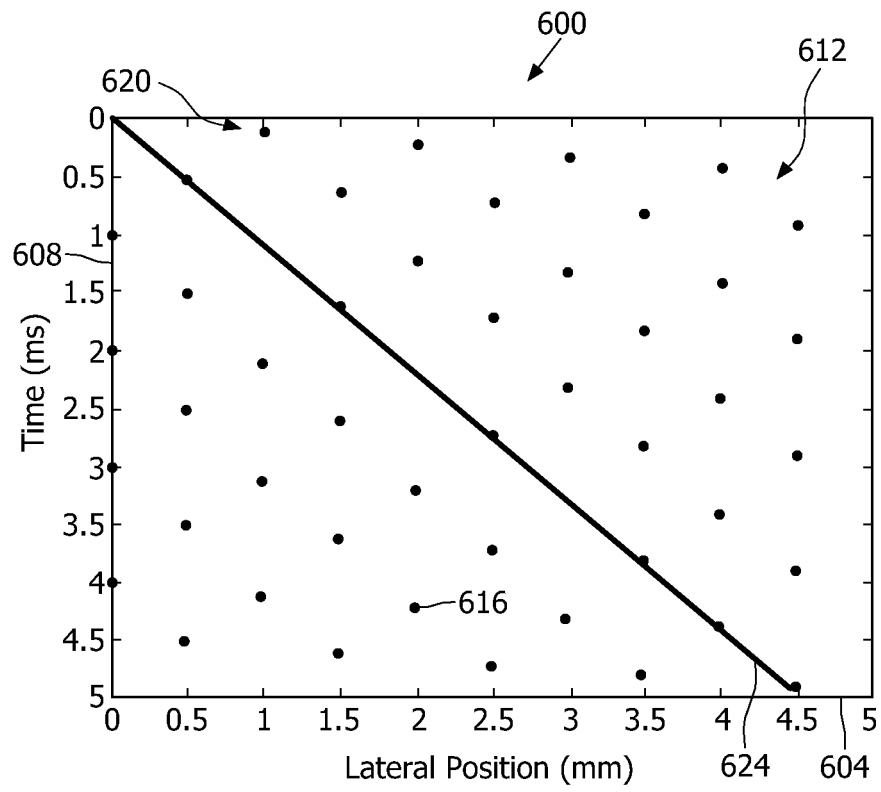


FIG. 6

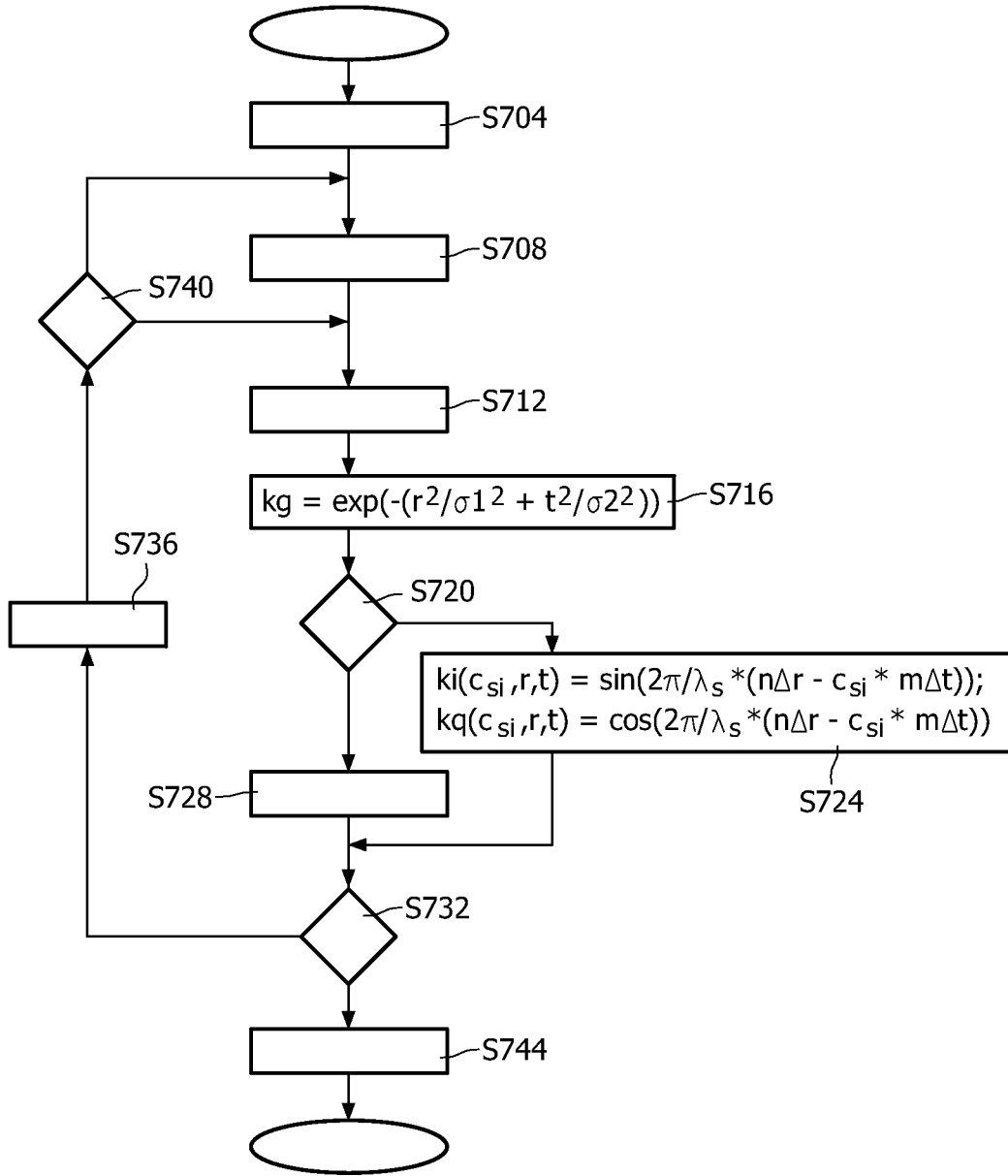


FIG. 7

REFERENCES CITED IN THE DESCRIPTION

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Patent documents cited in the description

- US 20040167403 A [0010]
- US 20090069693 A, Burcher [0059]

Non-patent literature cited in the description

- **C. PASSMANN ; H. ERMERT.** A 100-MHz ultrasound imaging system for dermatologic and ophthalmologic diagnostics. *IEEE Trans. Ultrasonics, Ferroelectrics and Frequency Control*, 1996, vol. 43 (4), 545-52 [0059]

专利名称(译)	空间 - 精细剪切波色散超声波振动测量采样		
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申请号	EP2010740738	申请日	2010-06-23
[标]申请(专利权)人(译)	皇家飞利浦电子股份有限公司		
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摘要(译)

在一些实施例中，实施剪切波散射超声波振动测量 (SDUV)，以从单个跟踪脉冲形成并行定向的接收线 (411-426)，用于测量单色剪切波。在一些实施例中，通过在位置上的通过，以隔行模式 (600) 在空间位置上执行采样，以进行波的测量。在一些实施例中，对波进行测量并且对测量应用一组滤波器 (S724)，其被调谐到相应的候选波速，所有这些都不需要确定不同空间位置处的波相之间的差异 (451-454)。

