



(12) **EUROPEAN PATENT APPLICATION**
published in accordance with Art. 158(3) EPC

(43) Date of publication:
09.10.2002 Bulletin 2002/41

(51) Int Cl.7: **A61B 8/00**

(21) Application number: **01900686.5**

(86) International application number:
PCT/JP01/00111

(22) Date of filing: **12.01.2001**

(87) International publication number:
WO 01/050961 (19.07.2001 Gazette 2001/29)

(84) Designated Contracting States:
**AT BE CH CY DE DK ES FI FR GB GR IE IT LI LU
MC NL PT SE TR**

- **MIWA, Yuichi**
Kokubunji-shi, Tokyo 185-8601 (JP)
- **BABA, Hirota**
Kashiwa-shi, Chiba 277-0005 (JP)

(30) Priority: **12.01.2000 JP 2000003727**

(74) Representative: **Strehl Schübel-Hopf & Partner**
Maximilianstrasse 54
80538 München (DE)

(71) Applicant: **Hitachi Medical Corporation**
Tokyo 100-0047 (JP)

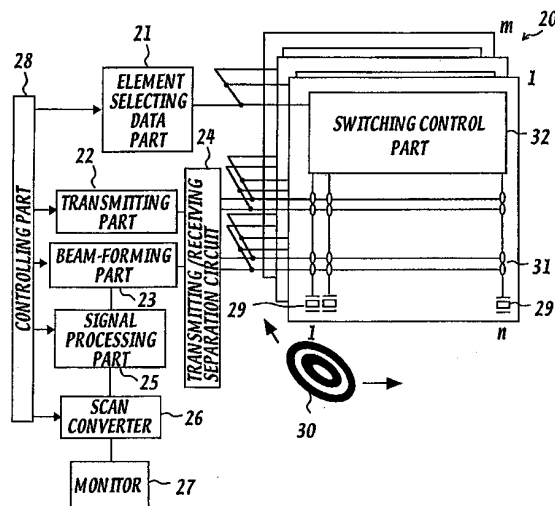
(72) Inventors:
• **SHINOMURA, Ryuichi**
Higashimatsuyama-shi, Saitama 355-0004 (JP)

(54) **ULTRASONIC DIAGNOSING APPARATUS**

(57) The present invention discloses an ultrasonic diagnostic apparatus that transmits an ultrasonic beam into an object to be examined by a multi-ring formed with transducer elements arrayed two-dimensionally in concentric rings and receives the echo so as to create a tomogram or a three-dimensional image of the object. To correct the focusing error due to the difference of ultrasound propagating paths, said ultrasonic diagnostic apparatus comprises a probe including two-dimensional array transducer elements for transmitting/receiving an ultrasonic to/from the object, means for grouping the

transducer elements so as to form a multi-ring, means for transmitting/receiving an ultrasonic beams with applying a delay to each ring of the multi-ring and scanning the ultrasonic beam so as to create said ultrasonic image, means for measuring the delay error due to sound speed non-uniformity portion of the object and changing at least either the coupling of the multi-ring or the delay time based on the measurement error and transmitting/receiving the ultrasonic beam, and means for imaging the inside of the object by scanning of corrected ultrasonic beam.

Fig.1



Description

FIELD OF THE INVENTION

[0001] The present invention relates to an ultrasonic diagnostic apparatus for acquiring an ultrasonic image of a diagnostic part by scanning the interior of an object to be examined in real time with an ultrasonic beam formed with two-dimensional array transducer, particularly to the ultrasonic diagnostic apparatus for correcting a focusing error due to a difference of propagating paths of ultrasound transmitted/received with multi-ring type transducer of which plural number of transducers are bundled into concentric rings.

BACKGROUND OF THE INVENTION

[0002] An apparatus having plural number of transducer composed of two-dimensional array transducer and sector scanning an ultrasonic beam (to arbitrary direction) generated with a transmitting/receiving diameter composed with a whole two-dimensional transducer is known. In this ultrasonic diagnostic apparatus, for example if 64×64 transducers are arrayed in two-dimensional, then all transducer number is 4,096. And an ultrasonic scanning is performed with separately delay control to each transducer element. In this case, a beam-forming circuit with 4,096 channels is necessary. Realizing of the beam-forming circuit having these multi-channel delay circuits is difficult. So by thinning out a driven element for forming one ultrasonic beam, channel number of delay circuit in the beam-forming circuit is reduced. But S/N of signal acquired by thinning out elements for driving is deteriorated. So said apparatus is realized by comprising a beam-forming circuit having delay channel number as many as possible. For example, there is an example of apparatus that comprises a beam-forming circuit having delay circuit of 256 channels for transmitting and 256 channels for receiving.

[0003] As shown in Fig.4, a linear scanning expanded a field of view by moving transmitting/receiving diameter in transducer elements 1 arrayed in two-dimensional in X, Y direction, and a scanning method applied a convex scanning to two-dimension are proposed. In this case, number of transducer element 1 is more than said sector scanning type apparatus. So for reducing channel number in the beam-forming circuit, an apparatus that forms ultrasound transmitting/receiving diameter 2 by composing of a multi-ring bundled plural number of transducer element 1 in two-dimensional array with concentric rings, and gives a consistent delay time to transducer elements composing one ring of said multi-ring, and transmits/receives an ultrasonic beam with applying a delay time between rings, and forms an ultrasonic image by moving said diameter 2 to X, Y directions is known.

[0004] As shown in Fig.5, in said multi-ring each ring is formed by bundling in concentric rings into transducer

elements of which distance from one focal spot F is almost the same L_1, L_2, \dots . And the diameter of most exterior ring is diameter 2 for ultrasound transmitting/receiving. In this method, the bundled transducer element in concentric rings is able to reduce greatly the number of channel in beam forming circuit, which is the number of delay circuit. And S/N of signal acquired by using all elements in diameter can be improved.

[0005] And in case of considering the shape of an ultrasonic beam, focusing calculation of an ultrasonic beam in the object to be examined is traditionally performed under the condition that sound speed in an ultrasonic propagation medium is uniform. As shown in Fig.6, traditional apparatus comprises receiving delay circuit 4, 4, ... comprising per transducer element of probe 3 having plural number of transducer and adder 5 for adding receiving signals output from these receiving delay circuit 4, 4, ... Although reflected signals from focus point 6 in the object reach to each transducer element to propagate medium 7, the difference of path length from the focus point to each transducer element causes difference in arrival time. In this case, said reflected signals reach early to transducer elements located in the center of probe 3, on the other hand reach late to transducer elements in the end of it. So the phase of wave surface 8 in receiving signal is not the same. Then the receiving signals output from transducer elements in the center part of probe are delayed with a large amount of delay time in receiving delay circuit 4 corresponding to said each receiving signal, and receiving signals output from transducer elements at the ends of probe are delayed with a small amount of delay time, and those signals are output to adder 5. With these delay operations, wave surface 9 of receiving signal output from receiving delay circuits 4 is the same phase. The receiving signal having the same phase such as wave surface 9 in this condition is added in adder 5 to be formed receiving signal 10.

[0006] But actually as shown in Fig.7, sound speed non-uniformity part 11 exists on course from the focus point 6 in the object to probe 3, so the wave surface of receiving signal is disturbed as shown in sign 8'. In this case, performing the delay operation assuming as the sound speed to be uniform, the wave surface of receiving signals output from receiving delay circuit 4 is distorted as shown in sign 9', and it is not the same phase. Accordingly the output added in adder 5 dose not grow in intensity, and its intensity is small such as receiving signal 10'.

[0007] To the Contrary, there is a technology referred to an adaptive ultrasonic imaging method to correct a delay amount in said receiving delay circuit 4 in accordance with sound speed in the medium. As the adaptive ultrasonic imaging technology, a mutual correlation method for correcting a delay amount by correction procession of a received signal between adjacent channels respectively, and a maximum value brightness method for searching a brightness maximum with changing a

delay amount of receiving delay circuits are known.

[0008] Fig. 8 shows a block diagram describing the mutual correlation method. In Fig.8, received signal from each transducer element, which is not shown in the figure, is delayed a predetermined amount with each receiving delay circuit 4, 4, ... This delay is possible by an analog delay circuits or a digital delay circuits. In this case, when an output of adjacent channels in each transducer element is performed a mutual correlation processing with correlation device 12, the phase difference between output of adjacent channels can be obtained. Then detecting the value, and transforming it to focus data in correction processing part 13, and feed back inputting the transformed data to focus controlling part 14, a delay amount is corrected with receiving delay circuits 4.

[0009] Fig. 9 is a block diagram for describing said maximum value brightness method. In Fig. 9, a received signal from each transducer element, which is not shown in the figure, is delayed in receiving delay circuits 4, 4, ... with a predetermined amount. The output delayed in receiving delay circuits 4, 4, ... is added in adder 5. And its output is input to maximum value detecting part 15. This maximum value detecting part 15 compares the input signal with the last input value. And in case the input value is smaller than the last value, focus data is slightly changed systematically in focus controlling part 14. And the output after phasing of echo signal received with changing this focus data is inputted to maximum value detecting part 15, and judged again. And after repeating this operation consecutively, when the detected value should converge at maximum value, its data is used as focus data

[0010] However as shown in Fig.4 and Fig.5, in an ultrasonic diagnostic apparatus formed transmitting/receiving diameter 2 by bundling two-dimensional array transducer element 1 in concentric rings to compose multi-ring, in case that there is a sound speed non-uniformity part 11 on the path from focus point 6 to probe 3 in the object, as transducer element 1 in two-dimensional array are bundled in concentric rings as thus described, so. it was difficult to detect the phase difference due to said path difference for correcting an influence of said sound speed non-uniformity part 11. Therefore, the phase difference of echo signals caused by said path difference with existence of sound speed non-uniformity part 11 is not corrected. As a result, an image quality is deteriorated because ultrasonic beam becomes worse.

[0011] Thus the present invention is to deal with these problems. And the purpose of the present invention is to provide an ultrasonic diagnostic apparatus being able to correct a focusing error by detecting the phase difference of echo signal due to the difference of ultrasonic propagating path, even its multi-ring is composed by bundling two-dimensional array transducer elements in concentric rings.

DISCLOSURE OF THE INVENTION

[0012] To achieve said object, an ultrasonic diagnostic apparatus of the present invention, which has a probe comprising plural number of transducer element arrayed in two-dimensional for transmitting/receiving an ultrasound to an object to be examined, and forming a diameter for ultrasound transmitting/receiving by bundling said two-dimensional array transducer elements in concentric rings to compose multi-ring, and transmitting/receiving an ultrasound with the application of delay between each ring in said multi-ring, and forming an ultrasonic image by scanning said beam, comprises means for measuring a focusing error due to a sound speed non-uniformity in said object and transmitting/receiving an ultrasonic beam corrected based on its measuring error by changing at least one of the bundling of said multi-ring or the delay time, and means for imaging the object by using an echo signal of the corrected ultrasonic beam.

[0013] And in the apparatus of the present invention, the diameter having multi-ring bundled in concentric rings two-dimensional array transducer element in said probe is divided into plural number of section in radial form from the center to the outer. And focusing error due to sound speed non-uniformity in the object is measured between this diameter of each divided section and between each section, and corrects the ultrasonic beam is corrected by feed backing this measured value to delay circuits.

[0014] Furthermore, in the apparatus of the present invention, the bundled diameter that is different from that of said multi-ring composed by bundling said transducer element of two dimensional array in said probe in concentric rings is formed. And focusing error due to sound speed non-uniformity in the object between each diameter is measured, and the ultrasonic beam is corrected by feed backing this measured value to delay circuits and returning the form of multi-ring to initial setting.

BRIEF DESCRIPTION OF THE DRAWINGS

[0015]

Fig.1 is a block diagram of the whole composition showing an embodiment of ultrasonic diagnosing apparatus according to the present invention.

Fig.2 is an explanation view of a probe showing the first embodiment of the present invention.

Fig.3 is an explanation view of a probe showing the second embodiment of the present invention.

Fig.4 is a plan view showing the embodiment in which a multi-ring is set to probe in the present invention or a traditional ultrasonic diagnostic apparatus, and transmitting and receiving of ultrasonic beam and two-dimensional scanning are performed.

Fig.5 is an explanation view showing a principal of

said multi-ring.

Fig.6 is an explanation view showing a formation of traditional ultrasonic beam.

Fig.7 is an explanation view showing the beam formation in case that a sound speed non-uniformity part is in medium when said ultrasonic beam is formed.

Fig.8 is a block diagram showing a composition for correcting delay amount by using a mutual correlation method for an adaptive imaging technology.

Fig.9 is a block diagram showing a composition for correcting delay amount by using a maximum value brightness method for an adaptive imaging technology.

THE BEST MODE FOR CARRYING OUT THE INVENTION

[0016] Hereinafter, an embodiment of the present invention will be explained in detail based on attached drawings.

[0017] FIG.1 is a block diagram of the whole composition showing an embodiment of ultrasonic diagnostic apparatus according to the present invention. This ultrasonic diagnostic apparatus forms an ultrasonic beam with two-dimensional array transducer, and acquires an ultrasonic image of diagnostic part in the interior of object to be examined by scanning an ultrasonic beam in real time. As shown in Fig.1, it comprises probe 20, element selecting data part 21, transmitting part 22, beam-forming part 23, transmitting/receiving separation circuit 24, signal processing part 25, scan converter 26, monitor 27, and controlling part 28.

[0018] Said probe 20 transmits an ultrasound to an object to be examined and receives its echo. It is composed of plural number of transducer element 29, 29, ... arrayed two-dimensionally. These transducer element 29, 29, ... are arrayed two-dimensionally such as 1~m in x direction and 1~n in y direction in planar view as shown in Fig.4. And said transducer elements arrayed two-dimensionally are bundled to compose a multi-ring in concentric rings, and the multi-ring forms ultrasonic transmitting/receiving diameter 30. A delay time is given between each ring of said multi-ring to transmit and receive the ultrasonic beam. The ultrasonic beam scanning is performed with moving said diameter 30 at each cycle of transmitting/receiving of ultrasound. And an ultrasonic image is formed. In addition, said multi-ring is made for example with fresnel-bundles.

[0019] In addition, to said vibrator 29, 29, ..., connection switch groups 31 are connected for coupling an arbitrary delay channel in beam-forming circuits described in later and transducer element. Furthermore, to this connection switch groups 31, switching control part 32 for controlling the switch operation is connected.

[0020] Elements selecting data part 21 memorizes elements selecting data to form transmitting/receiving diameter 30. And elements selecting data read out from

elements selecting data part 21 is transferred to switching control part 32. And by controlling said switching control part 32, switch on and off of connection switch groups 31 is controlled to form transmitting/receiving diameter 30.

[0021] Transmitting part 22 supplies a transmitting signal for an ultrasound emitting to ultrasonic transducer element respectively with the application of delay time such that the ultrasound transmitted from each transducer element which forms transmitting/receiving diameter 30 of said probe 20 is focused a desired focus point set in the object. And beam-forming part 23 performs a desired focusing procession respectively to a reflected echo signal received with transducer elements 29 of said probe 20 and forms a receiving beam by phasing and adding. And transmitting/receiving separation circuit 24 changes a connection of said transmitting part 22 and beam-forming part 23 to transducer elements 29, whether an ultrasound is transmitted or received.

[0022] Signal processing part 25 inputs the receiving signal from said beam-forming part 23 and obtains a data of one scanning line by processing such as detecting, compression, filtering processing, edge emphasizing etc. And scan converter 26 inputs the data from said signal processing part 25 and forms an image data for displaying to monitor 27, together performs scan conversion between ultrasonic scanning and scanning for display and interpolation processing of image data or the like. Furthermore, monitor 27 displays the data from said scan converter 26 as an ultrasonic image. And in the display screen, a three-dimensional image or an arbitrary slice image is displayed. And controlling part 28 controls an operation of said each composed element.

[0023] In the present invention, means for measuring a delay error in receiving signal due to sound speed non-uniformity part in said the object, and correcting one of said bundling of transducer elements in multi-ring or a delay time or both of them, is composed.

[0024] In the first embodiment, the diameter composed of multi-ring by bundling two-dimensional array transducer element 29, 29, ... of said probe 20 in concentric rings is divided into a plural number of region in radial form from the center to the outer. And between diameter of this divided each region, delay error (focusing error) due to sound speed non-uniformity part (refer to 11 in Fig.7) in the object is measured to correct beam.

[0025] The probe showing this first embodiment has transducer elements arranged two-dimensionally. And this is omitted in the figure, but actually they are arrayed with matrix in the direction of X and Y as same as shown in Fig.4. Said transducer elements are bundled into ring shape to form diameter of annular array (multi-ring). Its diameter is moved to X direction or Y direction as a cycle of transmitting/receiving for performing a linear scanning or a convex scanning ultrasonic beam, or a sector scanning beam without moving diameter. With these linear scanning, convex scanning, or sector scanning due to this two-dimensional probe, the image data of three-

dimensional volume is acquired from the object. This image data is taken into scan converter 26 and transformed to the image data. And it is displayed on screen of monitor 27 as an ultrasonic slice image or a three-dimensional ultrasonic image.

[0026] To make it simple, a basic diameter for acquiring one image is shown in Fig.2. In this Fig. 2, the diameter composed of multi-ring by bundling said two-dimensional array transducer element in concentric rings is divided into plural number of region in radial form from the center to the outer. For example, elements selecting data is transferred from elements selecting data part 21 shown in Fig.1 to switching control part 32. With the controlling of said switching control part 32, the dividing line L_1 , L_2 of crossing the center of said multi-ring are formed. And this divided line L_1 , L_2 divide multi-ring to four sectors Sa, Sb, Sc, Sd.

[0027] Said divided each sector Sa ~ Sd is respectively connected to transmitting part 22 and beam-forming part 23 as shown in Fig.1. And to multi-ring separated to each sector, the delay data calculated in the condition that sound speed is uniform in medium 7 (refer to Fig.6), is added. That is to say, in Fig.2, transmitting part 22 and beam-forming part 23 are connected respectively to ring a_1 , a_2 , a_3 , a_4 ; b_1 , b_2 , b_3 , b_4 ; c_1 , c_2 , c_3 , c_4 ; d_1 , d_2 , d_3 , d_4 divided into each sector Sa ~ Sd. And delay controlling is performed respectively. Accordingly, the ultrasonic beam is focused at some point with said delay.

[0028] At this time, if sound speed in medium 7 is consistent with sound speed when the delay data is calculated, then received signal grows with same phase adding because the phase of surface in received signal in after receiving phasing is the same phase as same as the case shown in Fig.6. In addition, if sound speed non-uniformity part 11 exists in medium 7, then received signal is small not to grow because the phase of surface in received signal in after receiving phasing is different each other as same as shown in Fig.7.

[0029] In the present invention, as shown in Fig.2, the multi-ring is divided into for example four sectors Sa~Sd, so the phase error (this corresponds to focusing error) is calculated with the correlation of received signal after receiving phasing between the channel of transducer elements in each divided sector and corrected as same as shown in Fig.8. That is to say, to received signal after said receiving phasing, the phase difference is calculated by mutual correlation between adjacent sectors in each ring divided into each sector Sa~Sd as shown in Fig.2. And the correlation processing is performed between each ring in each sector.

[0030] For example, in Fig. 2, in multi-ring divided into four sectors Sa~Sd, mutual correlation processing is performed between adjacent sectors such as a_1 and b_1 , b_1 and c_1 , c_1 and d_1 , d_1 and a_1 in the most interior ring. In addition, the mutual correlation processing is performed between adjacent sectors such as a_2 and b_3 , b_2 and c_2 , c_2 and d_2 , d_2 and a_2 in the second ring. Further-

more also in the third and the forth ring, the mutual correlation processing is performed between adjacent sectors. And to acquire relationship between each ring in each sector, the correlation processing between adjacent rings a_1 and a_2 , a_2 and a_3 , a_3 and a_4 in sector Sa is performed. And also in other sector Sb, the correlation processing is performed between adjacent rings b_1 and b_2 , b_2 and b_3 , b_3 and b_4 . Furthermore, also in other sector Sc, Sd, the correlation processing is performed between adjacent rings. In addition, a method of correlation processing is not restricted to the above described. Other method can be used.

[0031] On the other hand, it is preferable to correct the phase error by calculating delay amount that brings maximum lightness with changing delay amount of beam-forming part between channel of transducer elements in each divided sector in the same way as shown in Fig.9, in the condition that for example multi-ring is divided into four sectors Sa~Sd as shown in Fig.2. That is, it is preferable to correct the phase error by calculating the delay amount that brings maximum lightness with changing delay amount consecutively to ring, which is divided into each sector Sa~Sd, a_1 , a_2 , a_3 , a_4 ; b_1 , b_2 , b_3 , b_4 ; c_1 , c_2 , c_3 , c_4 ; d_1 , d_2 , d_3 , d_4 .

[0032] Next the second embodiment of the present invention will be described. In this second embodiment, it is preferable to form a bundled diameter being different from the diameter composed by bundling transducer elements arrayed two-dimensionally in said probe 20 to multi-ring in concentric rings, and measure delay error due to sound speed non-uniformity part in the object between each diameter (refer to 11 in Fig.7), and correct the beam.

[0033] Fig.3 is an explanation view of probe showing the second embodiment. This probe has two-dimensional array transducer elements. Each transducer element is connected to receiving delay circuit. And an ideal delay is given for some focus point to calculate delay error by correlating outputs of transducer elements. In the same way as shown in Fig.5, when multi-ring is bundled, if bundled transducer elements for forming one ring is formed for example that difference of reaching time (distance) of ultrasound to focus point F is in the range of $\lambda/10$ (λ is wave-length of ultrasonic beam), then the delay error is corrected with adding said calculated delay error to reaching time.

[0034] For example, it is assumed that a specified transducer element 33 has a delay error in multi-ring n1, n2, n3, n4 shown in Fig.3. Although transducer element 33 is bundled into ring n2 in ideal state, but when the delay error is added to it, the correction is performed such that it is bundled into ring n3. And the delay error is corrected. And after having calculated correction value of delay error, transducer element 33 is bundled to return the ring in original ideal state. Thus not the diameter for forming an ultrasonic beam actually (bundled ring n1~n4), but the delay error is detected with transducer elements in another bundled ring. And the correc-

tion is performed to make bundled ring with considering the delay error.

[0035] In case of the mentioned above, if a transmitter and a beam-forming circuits are connected to all of two-dimensional array transducer elements as shown in Fig. 3, then circuit scale is large. So for example it is preferable to bundle adjacent transducer elements into rectangular blocks, and connect the transmitter and the beam-forming circuits to bundled transducer elements as a unit. In addition also in the second embodiment, it is preferable to correct the phase error by calculating the delay amount in which output signal is maximum value with changing delay amount of beam-forming part as same as shown in Fig.9.

[0036] As thus described, the present invention comprises means for measuring a focusing error due to sound speed non-uniformity part in the object and correcting one or both of bundling or delay time of multi-ring having two-dimensional array transducer elements in concentric rings. And interior of the object is imaged with the corrected beam, so image quality of ultrasonic image is improved.

Claims

1. An ultrasonic diagnostic apparatus comprising a probe having two-dimensional array transducer elements for transmitting and receiving to an object to be examined, and forming a diameter for an ultrasound transmitting and receiving signal by bundling said two-dimensional array transducer elements to compose multi-ring in concentric rings, and transmitting and receiving an ultrasound beam with application of delay time between each ring of said multi-ring,

characterized in that

said ultrasonic diagnostic apparatus comprises means for transmitting and receiving ultrasonic beam corrected with said multi-ring by measuring focusing error due to sound speed non-uniformity interior of said object and modifying at least one of bundling of said multi-ring or delay time based on the measuring error, and means for imaging the object with echo signal of the corrected ultrasonic beam.

2. An ultrasonic diagnostic apparatus according to claim 1, wherein the diameter composed of multi-ring by bundling the two-dimensional array transducer elements of said probe in concentric rings is divided into plural number of section in radial shape from the center to the outer, and focusing error due to sound speed non-uniformity part in the object is measured between each section of this divided diameter or each section, and the ultrasonic beam is corrected by feeding back this measured value to delay circuits.

3. An ultrasonic diagnostic apparatus according to claim 1, wherein a bundled diameter being different from that of said multi-ring composed by bundling said two-dimensional array transducer elements of said probe in concentric rings, and the focusing error due to sound speed non-uniformity part in the object is measured between each diameter, and the ultrasonic beam is corrected by feeding back this measured value to delay circuits and returning the multi-ring to initial setting.

4. An ultrasonic diagnostic apparatus comprising;

probe having two-dimensional array transducer elements,
 transducer selection means for setting multi-ring transducers composed of plural number of ring to said two-dimensional transducer elements,
 means for dividing said set multi-ring to plural number of sections,
 means for calculating focusing error between sections in said set multi-ring,
 means for feed-back correcting said calculated focusing error to delay time set in said delay circuit,
 beam-forming part comprised delay circuits for applying delay time to each ring of said multi-ring transducers vibrator and adder circuit for adding an output of said each delay circuit,
 means for imaging the output signal of said beam-forming part.

5. An ultrasonic diagnostic apparatus according to claim 4, wherein means for calculating the focusing error between sections in said set multi-ring includes means for calculating the focusing error between rings in one section.

6. An ultrasonic diagnostic apparatus comprising;

transducer selection means for initially setting multi-ring transducers composed of plural number of ring to said two-dimensional array transducer elements,
 means for specifying transducer element having a focusing error in each ring of said multi-ring,
 ring correction means for building into said specified transducer element to different ring from said initial set ring,
 beam-forming part comprised delay circuits for applying delay time to each ring of said multi-ring and adder circuit for adding an output of said each delay circuit,
 means for imaging the output signal of said beam-forming part.

7. Ultrasonic diagnosing apparatus according to claim 6, wherein means for specifying transducer element having the focusing error includes means for bundling group of adjacent transducer elements different from ring and assigning a transmitter and beam-forming circuit to this bundled transducer group. 5

8. An ultrasonic diagnostic apparatus comprising;

transducer selection means for initially setting multi-ring transducer composed of plural number of ring to said two-dimensional array transducer elements, 10

means for setting multi-ring to calculate focusing error, separately from said multi-ring, 15

beam-forming part comprised delay circuits for applying delay time to respective ring of said multi ring transducer initially set or multi-ring for calculating said focusing error, and adder circuit for adding an output of said each delay circuit. 20

means for feed back correcting said calculated focusing error to said delay time,

means for imaging the output signal of said beam-forming part. 25

30

35

40

45

50

55

Fig.1

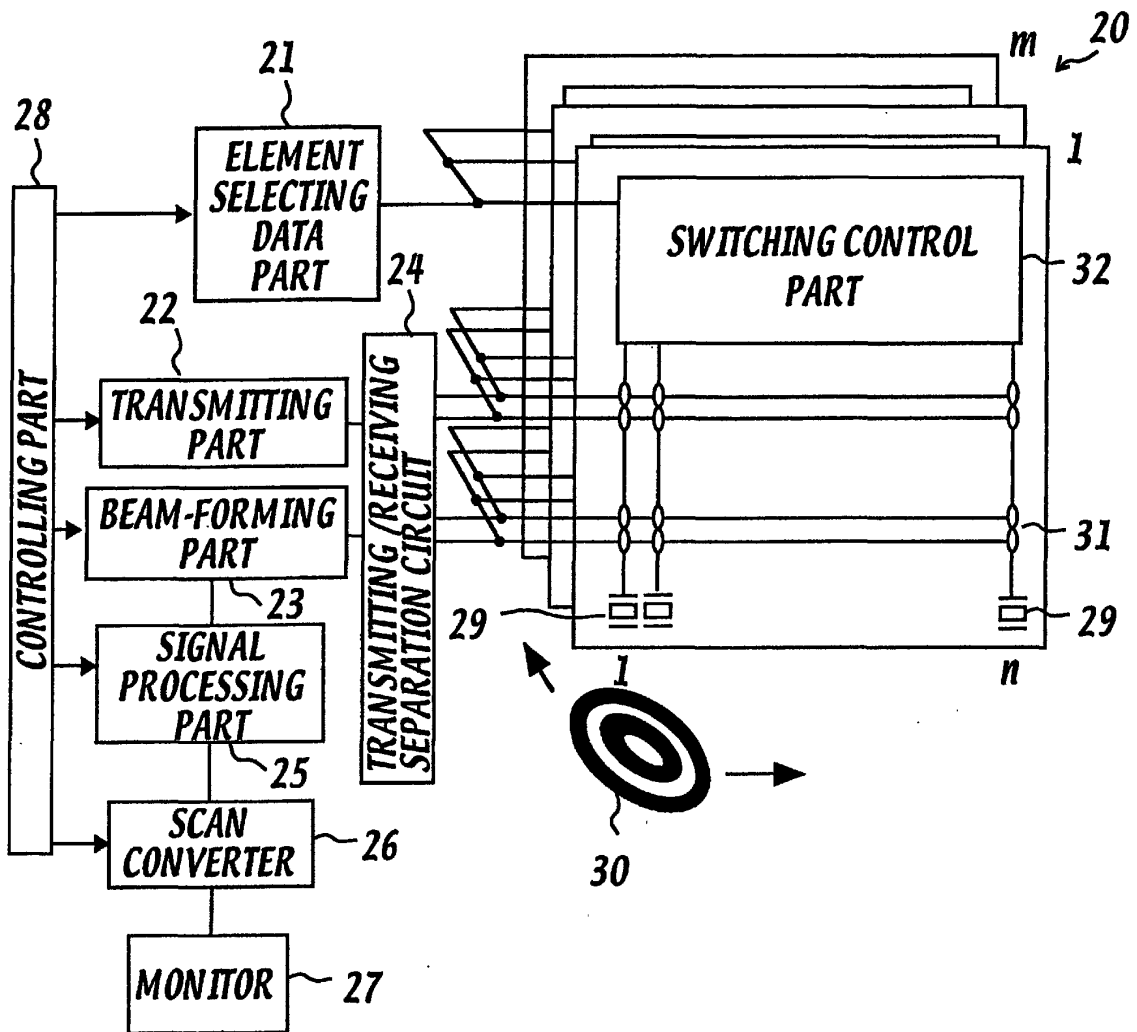


Fig.2

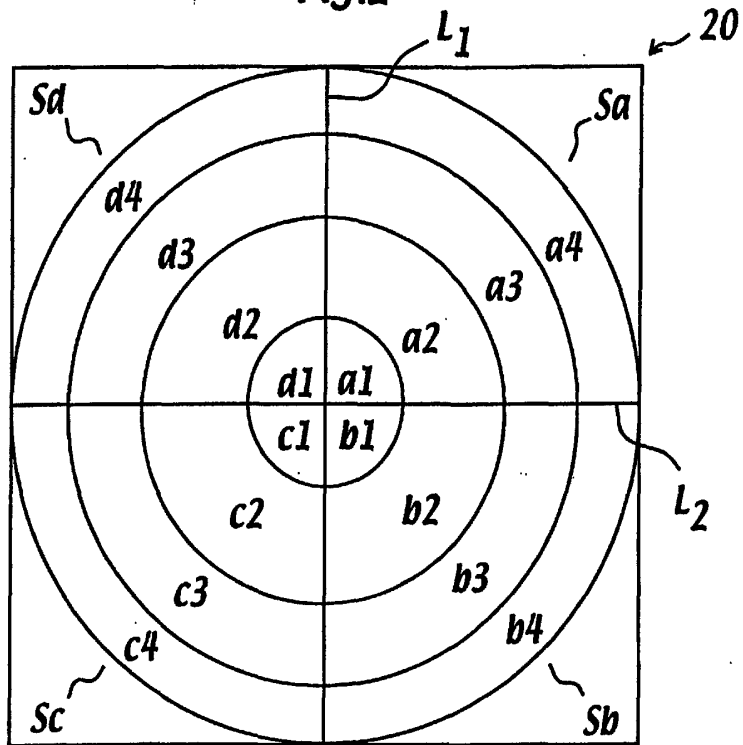


Fig.3

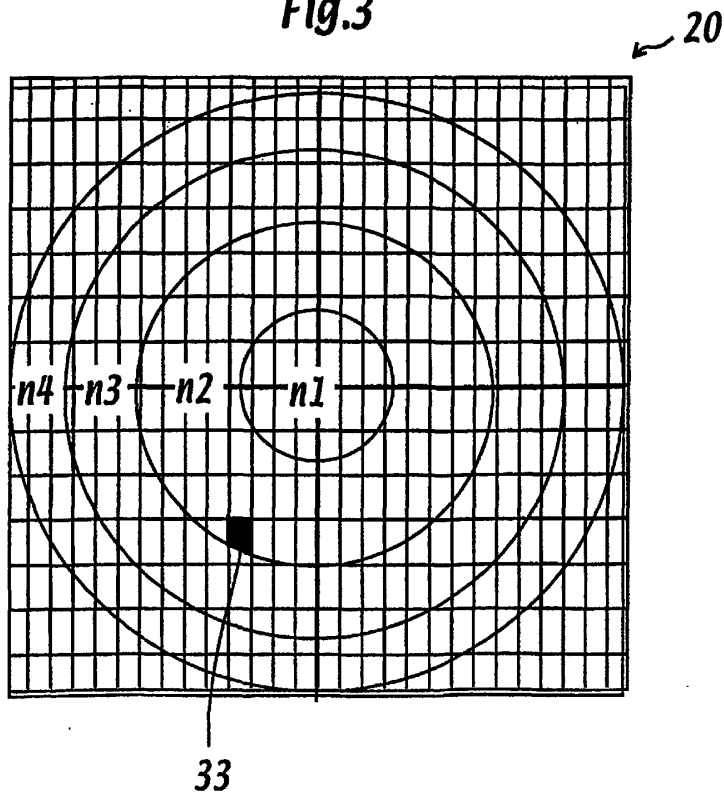


Fig.4

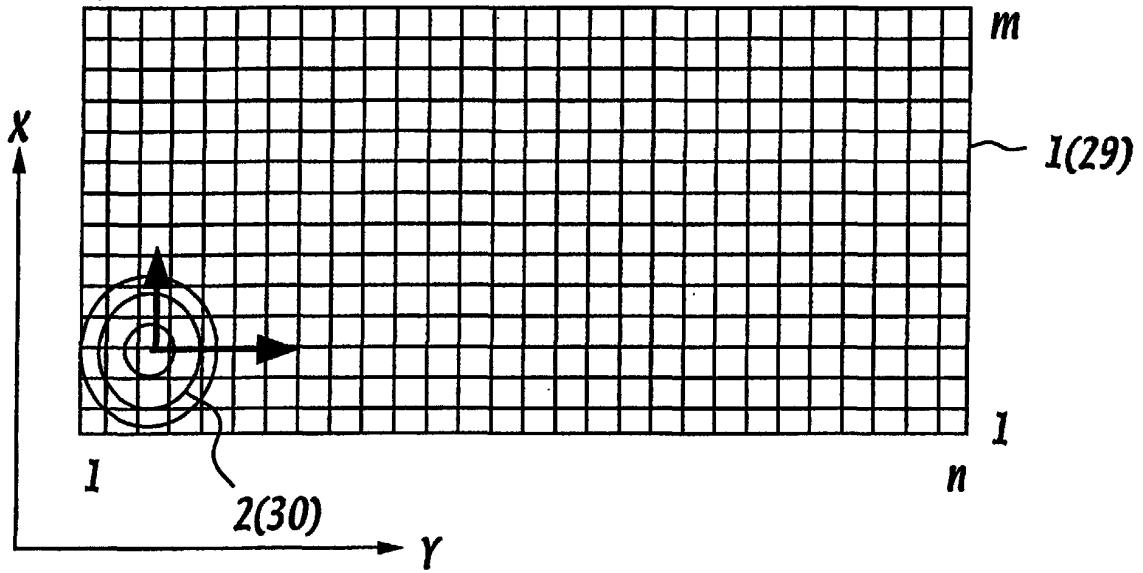


Fig.5

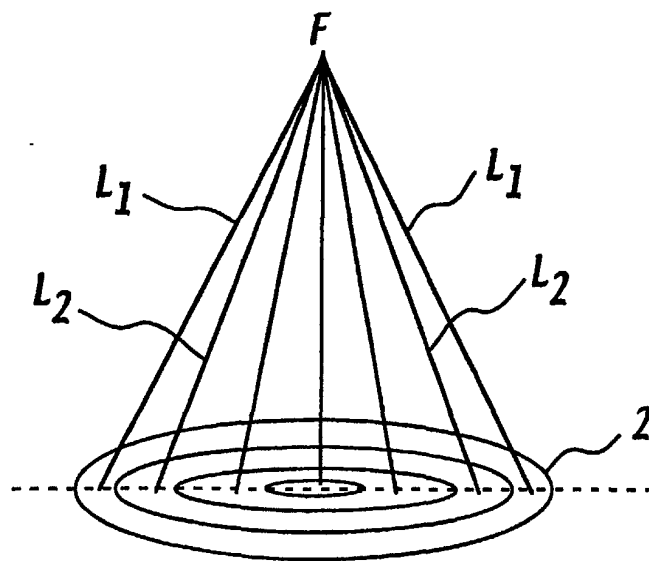


Fig.6

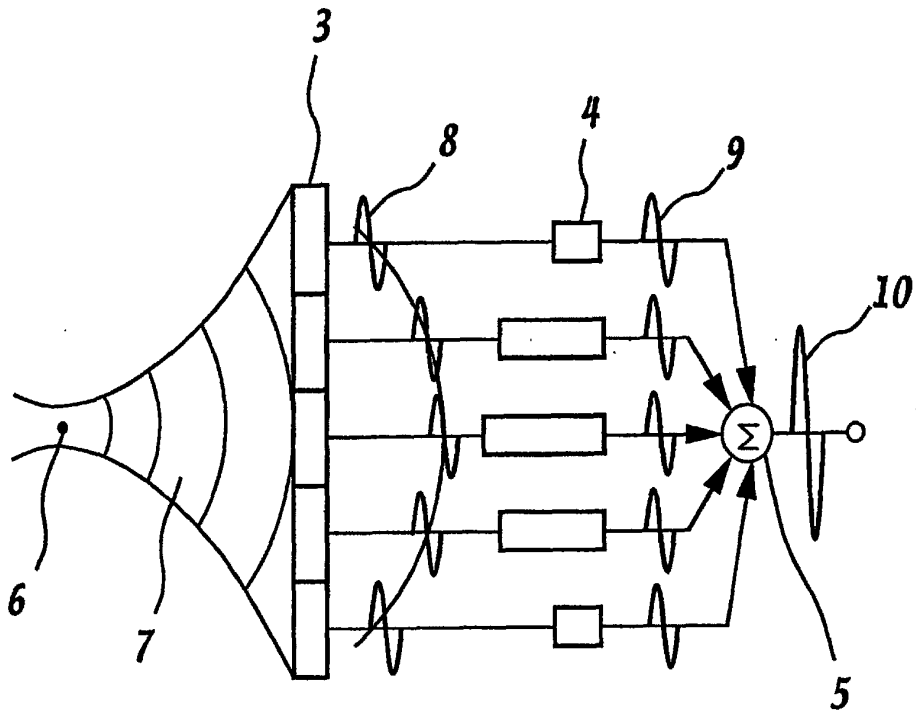


Fig.7

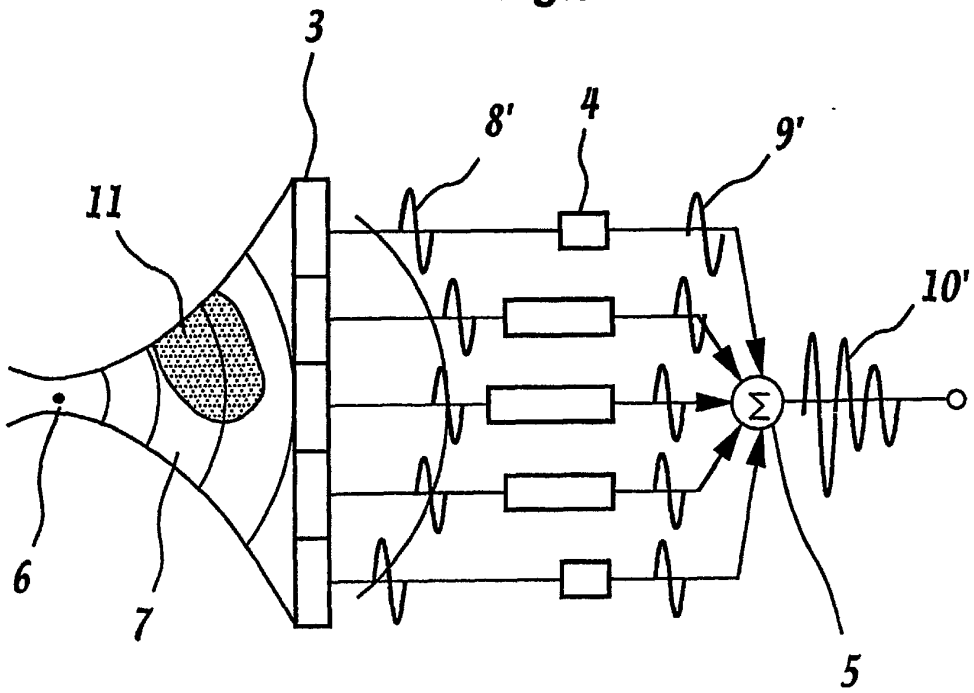


Fig.8

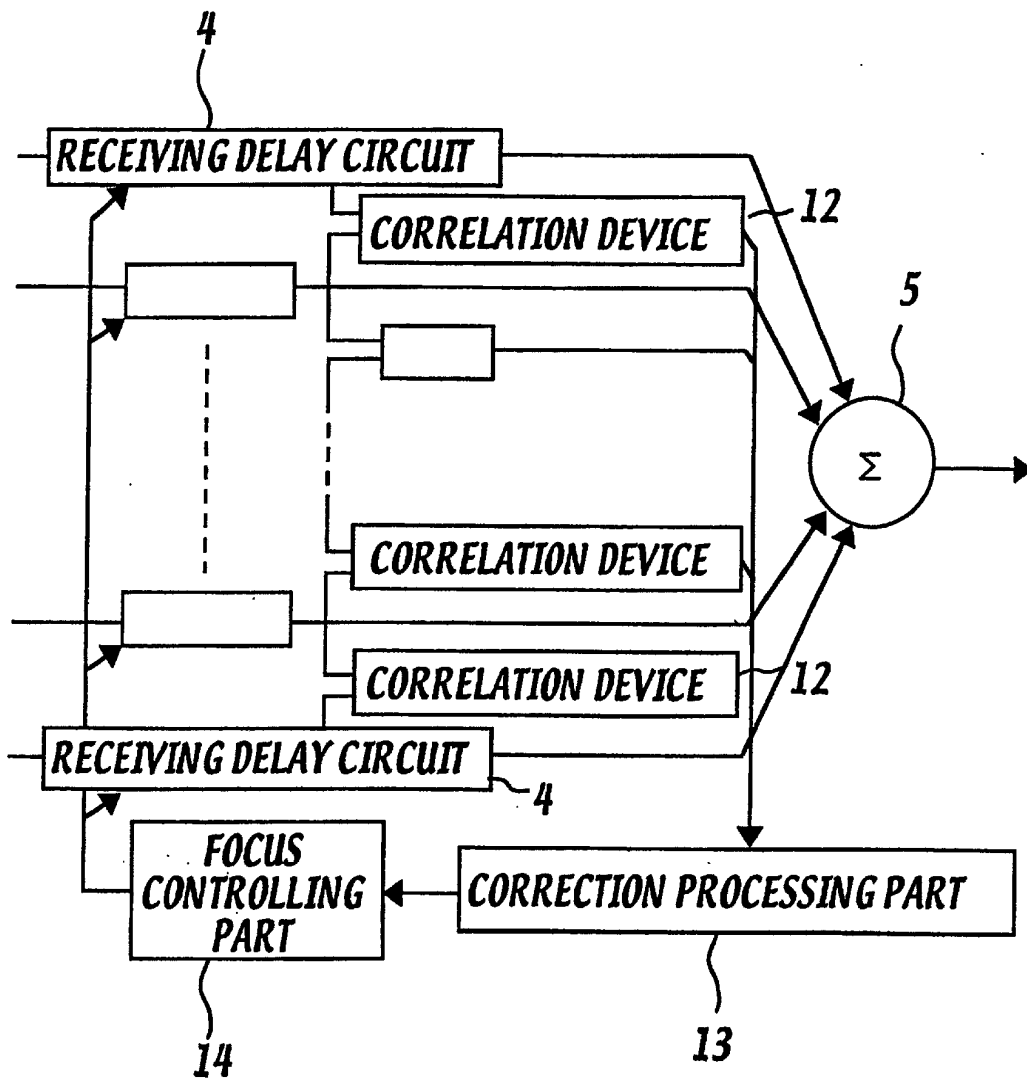
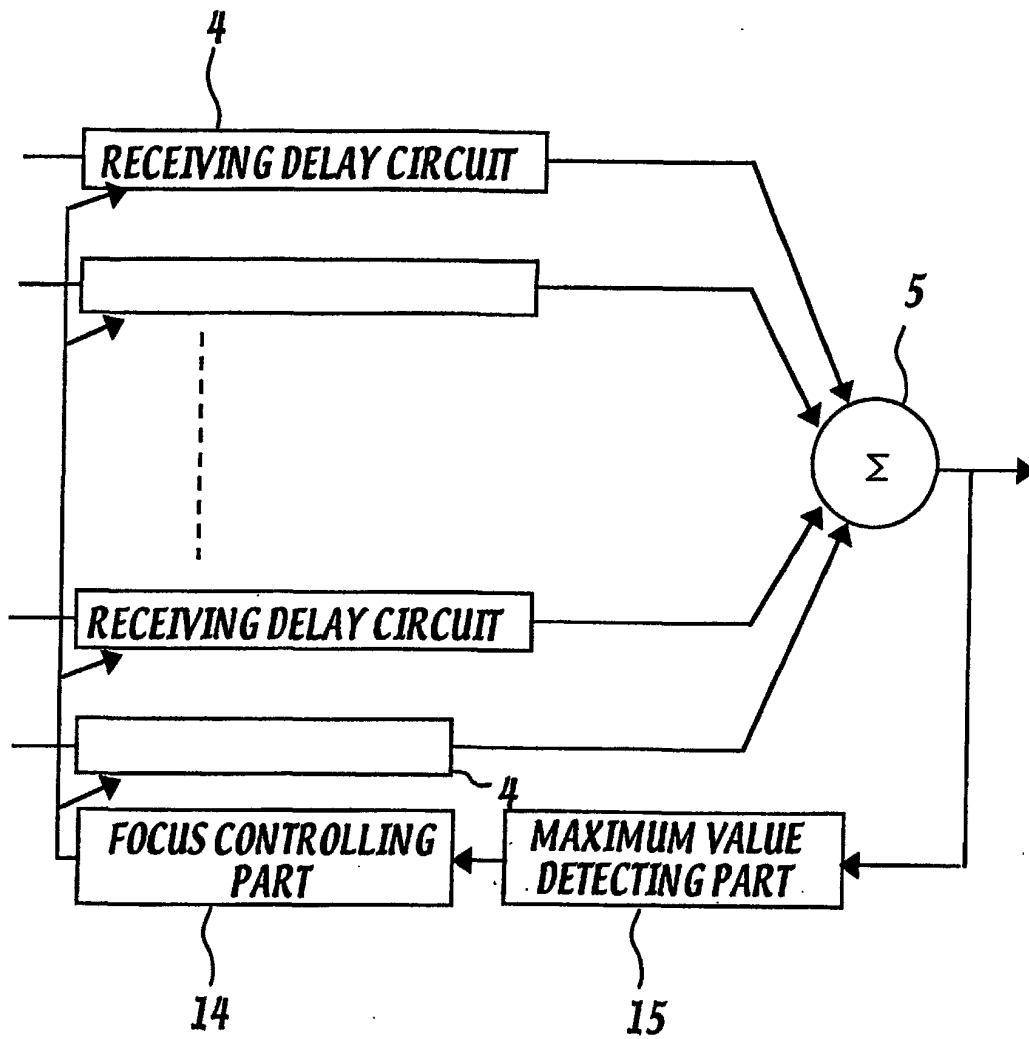


Fig.9



INTERNATIONAL SEARCH REPORT

International application No.

PCT/JP01/00111

A. CLASSIFICATION OF SUBJECT MATTER Int.Cl ⁷ A61B8/00		
According to International Patent Classification (IPC) or to both national classification and IPC		
B. FIELDS SEARCHED		
Minimum documentation searched (classification system followed by classification symbols) Int.Cl ⁷ A61B8/00-8/15		
Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched Jitsuyo Shinan Koho 1922-1996 Toroku Jitsuyo Shinan Koho 1994-2001 Kokai Jitsuyo Shinan Koho 1971-2001 Jitsuyo Shinan Toroku Koho 1996-2001		
Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)		
C. DOCUMENTS CONSIDERED TO BE RELEVANT		
Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
Y	US, 4641660, A (Robert Bele), 10 February, 1987 (10.02.87), Column 4, line 55 to Column 5, line 11; Fig. 1 & EP, 150634, A & FR, 2553521, A & JP, 60-150734, A	1, 4, 5, 8
Y	JP, 8-317923, A (Hitachi, Ltd.), 03 December, 1996 (03.12.96), Column 5, lines 10 to 44; Fig. 3 (Family: none)	1, 4, 5, 8
A	JP, 11-235341, A (Toshiba Corporation), 31 August, 1998 (31.08.98), Column 7, lines 35 to 44; Column 15, line 34 to Column 16, line 13 (Family: none)	1-8
A	Levin Nock et al, "Phase aberration correction in medical ultrasound using speckle brightness as a quality factor", THE JOURNAL of the Acoustical Society of America, Vol.85, No.5, 1989, pp.1819-1833 Full text; all drawings	1-8
<input type="checkbox"/> Further documents are listed in the continuation of Box C.		<input type="checkbox"/> See patent family annex.
* "A" "E" "L" "O" "P"	Special categories of cited documents: document defining the general state of the art which is not considered to be of particular relevance earlier document but published on or after the international filing date document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified) document referring to an oral disclosure, use, exhibition or other means document published prior to the international filing date but later than the priority date claimed	"T" "X" "Y" "&" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art document member of the same patent family
Date of the actual completion of the international search 29 January, 2001 (29.01.01)		Date of mailing of the international search report 06 February, 2001 (06.02.01)
Name and mailing address of the ISA/ Japanese Patent Office		Authorized officer
Facsimile No.		Telephone No.

Form PCT/ISA/210 (second sheet) (July 1992)

专利名称(译)	超声诊断仪		
公开(公告)号	EP1247490A4	公开(公告)日	2004-05-26
申请号	EP2001900686	申请日	2001-01-12
[标]申请(专利权)人(译)	株式会社日立医药		
申请(专利权)人(译)	日立医疗器械股份有限公司		
当前申请(专利权)人(译)	日立医疗器械股份有限公司		
[标]发明人	SHINOMURA RYUICHI MIWA YUICHI BABA HIROTAKA		
发明人	SHINOMURA, RYUICHI MIWA, YUICHI BABA, HIROTAKA		
IPC分类号	A61B8/00 B06B1/06 G01S7/52 G01S15/89 G10K11/34		
CPC分类号	G01S15/8925 A61B8/00 A61B8/4494 B06B1/0625 G01S7/52046 G01S7/52049 G01S15/8922 G01S15/8927 G10K11/346		
优先权	2000003727 2000-01-12 JP		
其他公开文献	EP1247490B1 EP1247490A1		
外部链接	Espacenet		

摘要(译)

一种超声诊断设备，该超声诊断设备借助于由二维排列并耦合到同心环中的振动器元件形成的多环将超声波束发射到对象体内，并接收回波以产生断层图或三维图像 被检体的图像，包括用于校正由于超声波传播路径的不同而引起的聚焦误差的探头，并且包括用于向/从被检体发送/接收超声波的二维排列的振子，用于对振子进行分组的装置 为了形成多环，用于对多环的每个环赋予延迟，发送/接收超声波束并扫描超声波束以产生超声波图像的装置，用于在a处测量延迟误差的装置。 主体中声速不均匀的部分，并根据测量误差至少改变多环的耦合或延迟时间，从而 发射/接收超声波束，以及用于通过校正后的超声波束对被检体内成像的装置。