

(19)



(11)

EP 2 454 998 B1

(12)

EUROPEAN PATENT SPECIFICATION

(45) Date of publication and mention
of the grant of the patent:

31.12.2014 Bulletin 2015/01

(51) Int Cl.:

A61B 8/12 (2006.01)

A61B 8/00 (2006.01)

(86) International application number:

PCT/JP2011/066081

(21) Application number: **11814427.8**

(22) Date of filing: **14.07.2011**

(87) International publication number:

WO 2012/017797 (09.02.2012 Gazette 2012/06)

(54) **ULTRASONIC DIAGNOSIS DEVICE**

ULTRASCHALLDIAGNOSEVORRICHTUNG

DISPOSITIF DE DIAGNOSTIC À ULTRASONS

(84) Designated Contracting States:

**AL AT BE BG CH CY CZ DE DK EE ES FI FR GB
GR HR HU IE IS IT LI LT LU LV MC MK MT NL NO
PL PT RO RS SE SI SK SM TR**

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(30) Priority: **06.08.2010 JP 2010177876**

(43) Date of publication of application:

23.05.2012 Bulletin 2012/21

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Description

Technical Field

[0001] The present invention relates to an ultrasound diagnostic apparatus that generates an ultrasound tomographic image by using ultrasound.

Background Art

[0002] Conventionally, ultrasound probes that use piezoelectric elements have been known, but in recent years, ultrasound probes that use broadband capacitive ultrasound transducers (called the C-MUTs) have been developed.

[0003] For example, as disclosed in Japanese Patent Application Laid-Open Publication No. 2008-516683 as a first conventional example, an ultrasound diagnostic apparatus that can be used by being connected with such ultrasound probes has been proposed. The C-MUT has a cavity on a silicon substrate and electrodes are provided over and under the cavity.

[0004] Bias voltages as well as ultrasound drive signals are applied onto these electrodes to vibrate a film at the top of the cavity, thereby transmitting ultrasound, and an echo signal that comes back is detected by the film at the top, so that the transmission and the reception of the ultrasound are achieved.

[0005] The C-MUT can be achieved using a MEMS (Micro Electro Mechanical Systems) process as well as the C-MUT can be smaller than a piezoelectric transducer because the size of one element is smaller. A technique has also been proposed in which the C-MUT, which can be smaller than a piezoelectric transducer, is connected with a drive shaft and used with an extra-fine ultrasound probe.

[0006] In addition, there are ultrasound diagnostic apparatuses that are implemented by arranging a plurality of ultrasound transducers and obtain ultrasound tomographic images by selecting some of the ultrasound transducers to perform transmission and reception. Such ultrasound diagnostic apparatuses need the same number of wirings as that of the selected ultrasound transducers.

[0007] To eliminate the wirings, International Publication No. 2001/021072, as a second conventional example, discloses a structure in which a multiplexer is implemented at a probe distal end part close to ultrasound transducers.

[0008] In the case of an ultrasound probe that mechanically rotates a C-MUT by means of a drive shaft as described above, when the probe is inserted into a thin lumen which is bent, followability of the drive shaft becomes poor in some cases, which causes its uneven rotation or the like and easy occurrence of image deletion or the like.

[0009] In addition, arranging a plurality of ultrasound transducers requires the same number of wirings as that of the elements of the ultrasound transducers. Thus, the

larger the number of the elements of ultrasound transducers is, the larger the outer diameter of the ultrasound probes becomes because of binding of the wirings. To solve this disadvantage, a solution has been proposed to arrange a multiplexer at a distal end portion of an ultrasound probe.

[0010] However, signal lines are required also for switching to select ultrasound transducers by a multiplexer as in the second conventional example. It is thus made difficult to apply a multiplexer to an ultrasound probe such as a catheter designed for use in a thin lumen.

[0011] For this reason, a configuration is desired that is applicable to broad purposes such as application to an ultrasound probe having a small outer diameter without a need for a new signal line for selecting ultrasound transducers, by utilizing transmission and reception signal lines for sending transmission and reception signals for ultrasound transmission and reception with respect to a plurality of ultrasound transducers also for the purpose of selecting ultrasound transducers that actually transmits and receives ultrasound.

[0012] US Patent Publication No. 20060084875 describes bias circuitry placed within an imaging device and used to apply a DC bias to one or more transducers requiring a DC bias to operate. The one or more transducers can be fabricated in a semiconductor manufacturing process and integrated with the bias circuitry on a common semiconductor substrate and further include a communication channel having two signal lines.

[0013] The present invention was made in view of the above-described points and it is an objective of the present invention to provide an ultrasound diagnostic apparatus that is applicable to broad purposes by utilizing transmission and reception signal lines also for the purpose of enabling to selectively drive ultrasound transducers to be used for actually transmitting and receiving ultrasound from a plurality of ultrasound transducers.

Disclosure of Invention

Means for Solving the Problem

[0014] The present invention is defined by the claims.

Brief Description of the Drawings

[0015]

Fig. 1 is an external view of an ultrasound diagnostic apparatus of a first embodiment of the present invention.

Fig. 2 is a block diagram illustrating a configuration of the ultrasound diagnostic apparatus of the first embodiment.

Fig. 3 is a diagram illustrating a part of an ultrasound transducer array in the first embodiment.

Fig. 4 is a block diagram illustrating a configuration of a signal determining portion.

Fig. 5 is a diagram illustrating a waveform of a transmission signal inputted into the signal determining portion.

Fig. 6 is an explanation diagram showing that a plurality of C-MUTs being a plurality of ultrasound transducers constituting the ultrasound transducer array are changed over so that the C-MUTs are driven to be electrically selected one after another and an explanation diagram of a conventional example in which one ultrasound transducer is mechanically driven to be rotated by a drive shaft to scan ultrasound.

Fig. 7 is a block diagram illustrating a configuration of an ultrasound diagnostic apparatus of a second embodiment of the present invention.

Fig. 8 is a diagram illustrating a part of an ultrasound transducer array in the second embodiment.

Fig. 9 is a block diagram illustrating a configuration of a signal determining portion.

Fig. 10 is a block diagram illustrating a configuration around a signal determining portion in a third embodiment of the present invention.

Fig. 11 is an explanation diagram of an operation of storing a selection signal into a look-up table (LUT) via a transmission and reception signal line in the third embodiment and an operation of mixing a clock for LUT with a transmission signal to select an ultrasound transducer.

Fig. 12 is a diagram illustrating a table of a set pattern A and a table of a set pattern B stored in the LUT.

Fig. 13 is a diagram illustrating a configuration around the signal determining portion in which the third embodiment is applied to three-electrode-type capacitive ultrasound transducers (C-MUTs).

Fig. 14 is a block diagram illustrating a configuration of an ultrasound diagnostic apparatus of a fourth embodiment of the present invention.

Fig. 15 is a diagram illustrating an example of a configuration around a signal determining portion in the fourth embodiment.

Best Mode for Carrying Out the Invention

[0016] Hereinafter, embodiments of the present invention will be described with reference to the drawings.

(First Embodiment)

[0017] Fig. 1 illustrates an external view of an ultrasound diagnostic apparatus 1 of a first embodiment of the present invention, and Fig. 2 illustrates an example of an internal configuration of the apparatus 1.

[0018] As shown in Fig. 1, the ultrasound diagnostic apparatus 1 includes an ultrasound probe 2 provided with an ultrasound transducer array, an ultrasound observing apparatus (hereinafter, simply referred to as the observing apparatus) 3 with which the ultrasound probe 2 is connected, and a monitor 4 as a display device that is

connected with the observing apparatus 3 and displays an ultrasound image.

[0019] The ultrasound probe 2 includes an elongated insertion portion 5 inserted into lumen, for example, blood vessels and the like, of an object to be examined, a grip portion 6 provided at a proximal end of the insertion portion 5, and a cable portion 7 extending from the grip portion 6. A connector 7A provided at an end portion of the cable portion 7 is detachably connected with a connector receiver (not shown) of the observing apparatus 3.

[0020] A distal end portion of the insertion portion 5 is provided with a plurality of ultrasound transducers, for example, an ultrasound transducer array 10 including a plurality of capacitive ultrasound transducers (Capacitive Micromachined Ultrasonic Transducers: abbreviated as the C-MUTs) 8a, 8b, 8c, ..., and 8n as shown in the enlarged view of Fig. 1. In the cylindrical insertion portion 5, the plurality of rectangular board shaped C-MUTs 8a, 8b, ..., and 8n are arranged so as to form an annular ring on an inner side of an exterior cover which allows ultrasound to pass through.

[0021] As shown in Fig. 2 and Fig. 3, the plurality of C-MUTs 8a, 8b, ..., and 8n constituting the ultrasound transducer array 10 are connected with a transmission and reception signal line 11A that sends transmission and reception signals and is inserted into the insertion portion 5 through signal determining portions 9a, 9b, ..., and 9n close to the plurality of C-MUTs 8a, 8b, ..., and 8n.

[0022] As shown in Fig. 2, the transmission and reception signal line 11A is connected with one end of a transmission and reception signal line 11B in the observing apparatus 3 through the connector 7A.

[0023] The transmission and reception signal line 11B is connected with a DC bias outputting portion 12 that outputs a direct current (DC) bias voltage (simply abbreviated as the DC bias) as well as the line 11B is connected with a transmitting portion 14 and a receiving portion 15 through a DC blocking portion 13 having a capacitor that blocks the DC bias.

[0024] The transmitting portion 14 includes a transmission signal outputting portion (or a transmission signal generating portion) 16 that outputs or generates transmission signals and a signal mixing portion (or a signal superimposing portion) 17 that mixes (or superimposes) the transmission signals with transducer selection signals (abbreviated as the selection signals) for selecting the C-MUTs 8i (i=a, b, ..., and n) used to transmit and receive ultrasound.

[0025] Further, a control portion 18 controls an output timing of a transmission signal outputted from the transmission signal outputting portion 16 and an output timing of a selection signal from the signal mixing portion 17. The signal mixing portion 17 mixes (superimposes), under the control of the control portion 18, each selection signal for selecting a transducer before an output waveform of each transmission signal.

[0026] That is, in the present embodiment, transmission signals to be generated have a signal form in which

selection signals in synchronization with the transmission signals are superimposed. The transmission signals on which the selection signals are superimposed are seen in Fig. 5 as described later.

[0027] The transmission signals on which the selection signals are superimposed are outputted from the transmitting portion 14. The DC biases from the DC bias outputting portion 12 are further superimposed on the transmission signals, and the transmission signals are transmitted to the transmission and reception signal line 11A of the ultrasound probe 2 via the transmission and reception signal line 11B. Then, the transmission signals sent via the transmission and reception signal line 11A are inputted into the signal determining portions 9i arranged at the distal end portion of the ultrasound probe 2.

[0028] In the present embodiment, in order to allow sequentially electrically driving the plurality of (n) C-MUTs 8a, 8b, ..., and 8n constituting the ultrasound transducer array 10 by n transmission signals, a selection signal for selecting each of the C-MUTs 8a, 8b, ..., and 8n is mixed (superimposed) before a signal waveform of each transmission signal.

[0029] Then, the signal determining portions 9i are provided on the transmission and reception signal line 11A that sends transmission and reception signals for transmitting and receiving the C-MUTs 8a, 8b, ..., and 8n, and the signal determining portions 9i determine by the selection signal whether or not the transmission and reception signal is for the C-MUTs 8i to be driven. The signal determining portions 9i then open or close a gate circuits 34i described later, in accordance with a result of the determination.

[0030] As seen from Fig. 2, a signal line inserted into the ultrasound probe 2 is only one transmission and reception signal line 11A except for ground lines (GND lines) connected with the ground (terminals), so that a structure suitable to reduce an outer diameter of the insertion portion 5 of the ultrasound probe 2 is achieved.

[0031] As shown in Fig. 2, the C-MUT 8i has an upper electrode 21i and a lower electrode 22i, and a cavity is made therebetween. The upper electrode 21i is connected with a ground (shown by G) through a signal line 23i and the lower electrode 22i is connected with one end of the signal determining portion 9i through a signal line 24i. The other end of the signal determining portion 9i is connected with the common transmission and reception signal line 11A.

[0032] The C-MUT 8i applies a transmission signal between the upper electrode 21i and the lower electrode 22i with a DC bias voltage applied, thereby vibrating a film facing the cavity, for example, a film at the upper electrode 21i side to transmit ultrasound. Also, if ultrasound is received with a DC bias applied, the film facing the cavity vibrates to generate an ultrasound reception signal as an electrical signal.

[0033] The reception signal is inputted into the receiving portion 15 in the observing apparatus 3 through the signal determining portion 9i. The reception signal is am-

plified by an amplifier portion 25 constituting the receiving portion 15 and then inputted into a reception signal processing portion 26. The reception signal processing portion 26 performs signal processing to generate an ultrasound tomographic image from the reception signal and outputs video signals of the ultrasound tomographic image generated in the signal processing to the monitor 4. On the display of the monitor 4 the ultrasound tomographic image is displayed.

[0034] The control portion 18 in the observing apparatus 3 also controls the DC bias outputting portion 12 and the reception signal processing portion 26. Also, an operation portion 19 is installed with which various operation signals are inputted to control the operation of the observing apparatus 3 through the control portion 18.

[0035] The present embodiment is the ultrasound diagnostic apparatus 1 including the plurality of C-MUTs 8a, 8b, ..., and 8n as a plurality of ultrasound transducers, and includes the transmission and reception signal line 11A that sends transmission and reception signals for transmitting and receiving ultrasound to and from the plurality of ultrasound transducers.

[0036] Also, the ultrasound diagnostic apparatus 1 includes signal determining portions 9a, 9b, ..., and 9n that are close to the plurality of ultrasound transducers and determine a selection signal for selecting an ultrasound transducer to be driven, the selection signal being sent out in synchronization with a transmission signal forming the transmission and reception signal, and electrically couple the ultrasound transducer to be driven to the transmission and reception signal line 11A in accordance with a result of the determination, and the transmission and reception signal line 11A sends the selection signal (mixed) with the transmission and reception signal.

[0037] In a third embodiment described later, a readout signal (a replacement for the selection signal) superimposed on the transmission signal is sent out and a signal determining portion 61 determines a CLK for LUT as a readout signal. Then, in accordance with the readout signal, data of the corresponding selection signal is read out from a selection look-up table portion in which the selection signals for selecting ultrasound transducers performing transmission and reception are prestored.

[0038] Fig. 3 illustrates an example of arrangement of C-MUTs 8i (Fig. 3 shows the case of i=a, b, c and d) and signal determining portions 9i. The signal determining portions 9i are contiguous to the C-MUTs 8i. It should be noted that the signal determining portions 9i may be integrated with the contiguous C-MUTs 8i. The respective signal determining portions 9i are provided on the common transmission and reception signal line 11A.

[0039] The signal determining portion 9i has a configuration as illustrated in Fig. 4. Fig. 5 illustrates a transmission signal (a transmission and reception signal) inputted into the signal determining portion 9i. The transmission signal forming the transmission and reception signal shown in Fig. 5 is generated under the control of the above-described control portion 18.

[0040] As seen from the following description, a transmission and reception signal includes a transmission signal in a selection code time period Ta and a transmission time period Tb shown in Fig. 5, and a reception signal in a reception time period Tc following the transmission time period Tb. Also, as seen from Fig. 5, the period for the transmission signal is time-divided into the selection code time period Ta and the transmission time period Tb, and a transducer selection code as a selection signal and a transmission signal are sent via the transmission and reception signal line 11A.

[0041] As shown in Fig. 5, a transmission signal inputted into the signal determining portion 9i via the transmission and reception signal line 11A includes the selection code time period Ta (as a selection signal time period) in which a pulse as a transducer selection code as a selection signal for selecting an ultrasound transducer to be driven that is actually used for transmission and reception is superimposed on a DC bias, and the transmission time period Tb having a transmission signal for driving the selected C-MUT 8i to be driven. Further, after the transmission time period Tb, only the DC bias is applied onto the transmission and reception signal line 11A, and the reception time period Tc starts in which a reception signal is received.

[0042] In the selection code time period Ta, a transducer selection code as a selection signal for determining the C-MUT 8i to be driven is inserted in, at a predetermined timing, before a waveform of transmission signal. As an example of the foregoing, as an example of a selection code signal inserted in the selection code time period Ta, Fig. 5 shows the case of a pulse having a predetermined pulse width.

[0043] As shown in Fig. 5, in the selection code time period Ta, in order to drive the first C-MUT 8a by a transmission signal, one pulse as a transducer selection code P1 corresponding to the first C-MUT 8a is time-divided and superimposed before a signal waveform of the transmission signal.

[0044] In this case, one pulse having a predetermined pulse width, for example, a negative pulse, is placed before the waveform of the transmission signal. After the transmission time period Tb and the reception time period Tc, in order to drive the second C-MUT 8b by the transmission signal, a transducer selection code P2 of two pulses is placed before a waveform of the transmission signal. Next to the transducer selection code P2 of two pulses, although not shown, transducer selection codes of three pulses, four pulses, ..., and n pulses follow.

[0045] The signal determining portion 9i shown in Fig. 4 includes a DC blocking and clipping circuit 31i into which the transmission signal is inputted and a gate circuit 34i.

[0046] The DC blocking and clipping circuit 31i includes a DC blocking circuit that blocks a DC bias component in a selection signal and a clipping circuit that clips a transmission signal with large amplitude to extract only a pulse that forms a selection signal with small am-

plitude. It should be noted that the DC blocking and clipping circuit 31i is not limited to a configuration in which a DC blocking circuit is integrated with a clipping circuit, and the DC blocking circuit may be separated from the clipping circuit.

[0047] A pulse (forming a selection signal) extracted by the DC blocking and clipping circuit 31i is inputted into a pulse counter 32i, and the pulse counter 32i counts the number of inputted pulses and outputs the number to a judging portion (or a determining portion) 33i.

[0048] The judging portion 33i judges (determines) whether or not the number agrees with a count number set beforehand in accordance with the C-MUT 8i contiguous to the signal determining portion 9i. For example, in a judging portion 33a contiguous to the first C-MUT 8a shown in Fig. 3, 1 is preset as a count number for judgment. Then, as shown in Fig. 5, if the transducer selection code P1 with the number of pulses being 1 is inputted, since the number of pulses agrees with the preset count number, the judging portion 33a judges that the transducer selection code P1 is a selection signal for selecting an ultrasound transducer to be driven which is used to transmit and receive ultrasound.

[0049] If the judging portion 33i judges that the code is a selection signal for driving the C-MUT 8i to be driven, the judging portion 33i applies a control signal to a gate opening and closing control terminal (simply referred to as the control end) of the gate circuit 34i to control the opening and closing of the gate of the gate circuit 34i, that is, to switch the gate from closed to open.

[0050] It should be noted that in Fig. 4, the DC blocking and clipping circuit 31i, the pulse counter 32i, the judging portion 33i, and the gate circuit 34i, which constitute the signal determining portion 9i, use the DC biases from the DC bias outputting portion 12 as an operating power supply.

[0051] For example, a DC bias is converted by a voltage converting circuit 35 in the signal determining portion 9i into a predetermined power supply voltage used to operate the pulse counter 32i, the judging portion 33i, and the gate circuit 34i. Then, the predetermined power supply voltage is supplied to the pulse counter 32i, the judging portion 33i, and the gate circuit 34i. The voltage converting circuit 35 is composed of a known three-terminal constant voltage integrated circuit (IC) (not shown).

[0052] In the present embodiment, because a DC bias is used as power supply, it is not necessary to insert a power supply line into the ultrasound probe 2 in order to operate the signal determining portion 9i. In other words, the transmission and reception signal line 11A also functions as a power supply line for sending power supply in order to operate the signal determining portion 9i.

[0053] It should be noted that in Fig. 4, although each signal determining portion 9i has a voltage converting circuit 35, for example, only one signal determining portion 9a may have a voltage converting circuit 35 and the voltage converting circuit 35 may supply power supply to the pulse counters 32a to 32n, the judging portions

33a to 33n, and the gate circuits 34a to 34n of all the signal determining portions 9a to 9n.

[0054] As described above, a transmission signal is inputted into (one terminal of) the gate circuit 34i, and if a control signal is applied from the judging portion 33i, the gate circuit 34i opens the gate. Then, the gate circuit 34i outputs a signal inputted into the one terminal of the gate circuit 34i to the other terminal.

[0055] In other words, the gate circuit 34i causes one terminal and the other terminal to enter a conductive state, that is, an electrically connected state in response to a control signal applied to a control end. In this case, a transmission signal offset by an inputted DC bias component is sent out to the C-MUT 8i. It should be noted that the gate circuit 34i is set to close when the gate circuit 34i receives a start signal of a next selection signal time period Ta.

[0056] Therefore, as shown in Fig. 5, if the gate circuit 34i is opened in the transmission time period Tb, the opened state is maintained for the reception time period Tc. That is, the gate circuit 34i is opened to send out a transmission signal to the C-MUT 8i to be driven as well as the gate circuit 34i maintains the open state to send out a reception signal received by the C-MUT 8i used for the transmission, to the observing apparatus 3 via the transmission and reception signal line 11A in the reception time period Tc.

[0057] Fig. 5 illustrates gate opening and closing of the gate circuits 34a and 34b as a specific example. It should be noted that an L level indicates closed and an H level indicates open. The transmission signal is applied onto the C-MUT 8i via the gate circuit 34i, and thereby the C-MUT 8i transmits ultrasound.

[0058] As described above, in the ultrasound transducer array 10, since the C-MUTs 8a, 8b, ..., and 8n are arranged to form an annular ring shape, and selection signals with the number of pulses set as 1, 2, ..., and n are placed before the transmission signals, the C-MUTs 8a, 8b, ..., and 8n are sequentially selected and driven by the transmission signals to radially transmit ultrasound (radially scan) by the driven C-MUT 8i.

[0059] Then, if the distal end portion of the ultrasound probe 2 is inserted in lumen sites in the object to be examined, such as a bile duct and a pancreatic duct, the C-MUT 8i radially transmit ultrasound to a duct wall around the distal end portion of the ultrasound probe 2. An ultrasound echo reflected from a part in which acoustic impedance is changed is received by the C-MUT 8i used for the transmission.

[0060] The received ultrasound echo is changed by the C-MUT 8i into an electrical reception signal and passes through the transmission and reception signal lines 11A and 11B. Then, the DC bias component of the electrical signal is blocked by the DC blocking portion 13 and the signal is inputted into the amplifier portion 25. After the amplifier portion 25 amplifies the reception signal, an ultrasound tomographic image from the radial scan is generated by the reception signal processing portion 26

and displayed on the monitor 4.

[0061] Fig. 6(A) illustrates a scheme in which the C-MUTs 8a, 8b, ..., and 8n constituting the ultrasound transducer array 10 in the present embodiment are sequentially changed over and driven to perform radial electronic scanning. Fig. 6(B) schematically illustrates a conventional example of a scanning scheme that uses a drive shaft 41.

[0062] As described above, the present embodiment adopts the scheme in which selection signals are superimposed on transmission signals and C-MUTs 8i to be driven are sequentially selected (changed over) by the selection signals to perform radial electronic scanning on ultrasound.

[0063] In the conventional example shown in Fig. 6(B), as an ultrasound transducer on the drive shaft 41, for example, a C-MUT 42 is mechanically driven to rotate in an arrow direction to mechanically scan ultrasound.

[0064] In the present embodiment, without the C-MUT 42 shown in Fig. 6(B) being mechanically driven to rotate, selected C-MUTs can be changed over one after another in an arrow direction of Fig. 6 (A), like 8a, 8b, 8c, and so on, to radially scan ultrasound and obtain an ultrasound tomographic image by the radial scanning.

[0065] As a result, according to the present embodiment, a flow of an image caused by the poor followability of the drive shaft 41 can be prevented from occurring, and an ultrasound tomographic image with high quality can be obtained.

[0066] Furthermore, in spite of such an electronic scanning scheme in which C-MUTs 8i are changed over and driven, the transmission and reception signal line 11A sends transmission and reception signals as well as functions as a signal line that sends selection signals.

[0067] Thus, according to the present embodiment, the ultrasound transducer array 10 can be driven by only one transmission and reception signal line 11A except for the ground lines, so that the number of signal lines inserted into the ultrasound probe 2 can be reduced.

[0068] Thus, according to the present embodiment, since the number of signal lines can be reduced, advantageously, the insertion portion 5 of the ultrasound probe 2 can be made thin, that is, an outer diameter of the insertion portion 5 can be reduced.

[0069] In addition, the present embodiment can be applied to use in which for example, the insertion portion 5 of the ultrasound probe 2 is made thin and inserted in thinner lumens. That is, the present embodiment can be widely applied.

(Second Embodiment)

[0070] Fig. 7 illustrates a configuration of an ultrasound diagnostic apparatus 1B of a second embodiment of the present invention. The ultrasound diagnostic apparatus 1B includes an ultrasound probe 2B, an observing apparatus 3B, and a monitor 4.

[0071] The C-MUT 8i in the ultrasound transducer ar-

ray 10 of the above-described first embodiment has two electrodes.

[0072] On the other hand, a plurality of C-MUTs 48a, 48b, ..., and 48n (in Fig. 7, simply denoted by the C-MUTs 48a, ..., and 48n) constituting an ultrasound transducer array 10B in the present embodiment include the following three electrodes: an upper electrode 21i, a lower electrode 22i, and a ground electrode (GND electrode) 49i being near the lower electrode 22i and connected with a ground.

[0073] A signal line 23i connected with the upper electrode 21i of the C-MUT 48i is connected with a transmission and reception signal line 11A through a signal determining portion 9i, and the lower electrode 22i is connected with a DC bias signal line 11A' inserted into the ultrasound probe 2B. The GND electrode 49i is each connected with the ground via a GND line 50i.

[0074] The transmission and reception signal line 11A is connected with a transmitting portion 14 and a receiving portion 15 via a transmission and reception signal line 11B in the observing apparatus 3B (without the DC blocking portion 13 of Fig. 2 being inserted) and the DC bias signal line 11A' is connected with a DC bias outputting portion 12 via a DC bias signal line 11B' in the observing apparatus 3B. The other components are the same as those in Fig. 2.

[0075] Thus, the C-MUT 48i in the present embodiment includes the upper electrode 21i to which transmission and reception signals are applied, the lower electrode 22i to which DC bias voltages are applied, and the GND electrode 49i set at the GND potential. The second embodiment is different from the first embodiment illustrated in Fig. 1 in the point that an electrode onto which DC biases are applied is different from an electrode onto which transmission and reception signals are applied.

[0076] Therefore, a transmission signal outputted from a transmission signal outputting portion 16 is mixed with a selection signal in a signal mixing portion 17, and sent out via the transmission and reception signal lines 11B and 11A to the signal determining portion 9i.

[0077] In the signal determining portion 9i, if a C-MUT 48i is selected, the transmission signal is sent out to the upper electrode 21i of the C-MUT 48i to cause a film at the upper electrode 21i to send out ultrasound.

[0078] The C-MUT 48i outputs a reception signal obtained from ultrasound caused by the transmission signal transmitting ultrasound and reflected from an object to be examined, to the receiving portion 15 via the signal determining portion 9i, and the transmission and reception signal lines 11A and 11B. The receiving portion 15 amplifies the reception signal by an amplifier portion 25, imaging the reception signal at a reception signal processing portion 26, and displays the reception signal on the monitor 4 as an ultrasound tomographic image.

[0079] Here, an example of arrangement relationship between three-electrode-type C-MUTs 48i and signal determining portions 9i is shown in Fig. 8. The signal determining portions 9a to 9d are on the transmission and

reception signal line 11A and are connected with the C-MUTs 48a to 48d, respectively.

[0080] The opposite side of the C-MUTs 48a to 48d is connected with the DC bias signal line 11A', which is connected with the lower electrodes 22a to 22d of the C-MUTs 48a to 48d and with the DC bias outputting portion 12. It should be noted that although not shown in Fig. 8, a GND line 50 connected with the GND electrode 49i is disposed contiguous to the DC bias signal line 11A'. Also, the DC bias signal line 11A' is connected with the signal determining portion 9i to supply power thereto (not shown).

[0081] A configuration of the signal determining portion 9i in the present embodiment is shown in Fig. 9. In the configuration of the signal determining portion 9i shown in Fig. 4, the DC blocking and clipping circuit 31i has been adopted in order to take a selection signal out of a transmission signal. On the other hand, the signal determining portion 9i in Fig. 9 is different from that in Fig. 4 in the point that the signal determining portion 9i does not have a DC blocking circuit part but uses a clipping circuit 51i that clips a waveform of a transmission signal with large amplitude and extracts a selection signal in order to take a selection signal out of a transmission signal.

[0082] In the case of the three-electrode-type configuration, because a DC bias component is not superimposed on a transmission signal, processing for DC blocking is not needed. Thus, the clipping circuit 51i may be a diode-like device. Further, a reception signal can be processed without being passed through the DC blocking portion 13 of the first embodiment, effects of the DC blocking portion 13 such as a capacitor (on a signal waveform at a low frequency side) can be reduced.

[0083] The other configurations and operations are the same as those in the first embodiment. Further, also in the present embodiment, because the transmission and reception signal line 11A also functions as a signal line that sends selection signals, the ultrasound transducer array 10 can be driven by using only one transmission and reception signal line 11A and one DC bias signal line 11A', except for the ground lines. Therefore, advantageously, the number of signal lines inserted into the ultrasound probe 2 can be reduced, so that the insertion portion 5 of the ultrasound probe 2 can be made thin, that is, an outer diameter of the insertion portion 5 can be reduced. Therefore, the present embodiment can be widely applied.

(Third Embodiment)

[0084] In the foregoing embodiments, the case has been described in which one C-MUT that is actually used for transmission and reception, i.e., only a single C-MUT is selected by a selection signal. In the present embodiment, the case in which a plurality of ultrasound transducers are selected at a time is described.

[0085] Fig. 10 illustrates a configuration of a signal de-

termining portion 61 in which for example, a plurality of C-MUTs (here, four C-MUTs 8a to 8d) in the ultrasound probe 2 shown in Fig. 1 can be selected by selection signals. It should be noted that the present embodiment can be applied in the same manner to the case of more than four C-MUTs.

[0086] As in the case described in the first embodiment, a common transmission and reception signal line 11A is connected with (a lower electrode 22i of) a C-MUT 8i via each gate circuit 34i, and (an upper electrode 21i of) each C-MUT 8i is connected with the ground via a signal line 23i.

[0087] In the first embodiment, each gate circuit 34i is opened and closed (more specifically, from closed to open) by a control signal from an individual signal determining portion 9i, but in the present embodiment, one selection circuit 62 controls the opening and closing of each of, for example, four gate circuits 34a to 34d.

[0088] In other words, in the present embodiment, the signal determining portion 61 includes the gate circuits 34a to 34d connected and contiguous to the C-MUTs 8a to 8d, and one selection circuit 62 that controls the gate opening and closing of the plurality of gate circuits 34a to 34d.

[0089] As shown in Fig. 10, the selection circuit 62 includes a DC blocking and clipping circuit 31, a look-up table (abbreviated as the LUT) 63 as a selection look-up table portion in which information of a selected C-MUT 8i is stored, and a timing generating oscillation portion (abbreviated as the OSC portion) 64 for operating the LUT 63.

[0090] It should be noted that as described below, the LUT 63 stores (data of) selection signals for selecting a C-MUT 8i to be driven before the C-MUT 8i is actually driven by a transmission signal.

[0091] Operations including the selection circuit 62 will be described using timing diagrams in Fig. 11. Fig. 11(A) illustrates a timing diagram for explaining an operation to store a transducer selection code 71 as a selection signal in the LUT 63 of the selection circuit 62 using, for example, the transmission and reception signal line 11A.

[0092] The observing apparatus 3 sends out a trigger 72 for a transducer selection code via the transmission and reception signal line 11A, and thereby the DC blocking and clipping circuit 31 of the selection circuit 62 judges that the transducer selection code 71 is sent out in synchronization with a timing that follows the trigger 72 for transducer selection code. Then, the DC blocking and clipping circuit 31 sends a judgement signal to the OSC portion 64, and the OSC portion 64 generates a timing signal for storing the transducer selection code 71 in the LUT 63.

[0093] The transducer selection code 71 sent out via the transmission and reception signal line 11A after the trigger 72 for transducer selection code is stored in the LUT 63 in synchronization with the timing signal of the OSC portion 64.

[0094] In this manner, the LUT 63 stores the data of

the transducer selection code 71 as a selection signal for selecting and driving the C-MUTs 8a to 8d. In the present embodiment, after the data of a selection signal is stored in the LUT 63 in such a manner, ultrasound is actually transmitted or received. For example, the transmitting portion 14 shown in Fig. 1 mixes a clock for LUT (abbreviated as the CLK for LUT) 73 as a readout signal for reading out a selection signal stored in the LUT 63, at a predetermined timing before a signal waveform of a transmission signal.

[0095] If the C-MUTs 8a to 8d are actually driven, the transmitting portion 14 prefixes the CLK 73 for LUT to a transmission signal shown in Fig. 11(B) and sends out the signal via the transmission and reception signal line 11A to the signal determining portion 61.

[0096] It should be noted that in the first embodiment, as shown in Fig. 5, the number of pulses of the transducer selection code has changed like P1, P2, and so on, but in the present embodiment, the same one CLK 73 for LUT is used.

[0097] In Fig. 11 (B), the CLKs 73 for LUT are placed instead of the transducer selection code in the selection code time period Ta of Fig. 5. Because also in the time period in which the CLKs 73 for LUT are placed, data of a selection signal is read out from the LUT 63 and an ultrasound transducer to be driven is selected by the read-out selection signal, the period is denoted as the selection signal time period Ta'.

[0098] Further, in Fig. 11 (B), the CLK 73 for LUT is placed at a timing position of the start of the reception time period Tc following the transmission time period Tb, and the C-MUTs 8a to 8d for receiving ultrasound in the reception time period Tc in synchronization with the timing of this CLK 73 for LUT are selectively set. That is, the first CLK 73 for LUT placed before the signal waveform of the transmission signal in the transmission time period Tb is used as a readout signal for selecting an ultrasound transducer for transmission and the second CLK 73 for LUT placed after the signal waveform of the transmission signal is used as a readout signal for selecting an ultrasound transducer for reception.

[0099] As shown in Fig. 11(B), if the CLK 73 for LUT placed before the signal waveform of the transmission signal is transmitted, the DC blocking and clipping circuit 31 sends a signal in synchronization with the timing of the CLK 73 for LUT to the OSC portion 64. The OSC portion 64 applies a clock corresponding to the CLK 73 for LUT onto the LUT 63.

[0100] In response to the application of the clock corresponding to the CLK 73 for LUT from the OSC portion 64, in accordance with the data of the selection signal stored in the LUT 63, the LUT 63 outputs a control signal for controlling the (gate) opening and closing of the gate circuits 34a to 34d contiguous to the C-MUTs 8a to 8d, respectively. Then, in accordance with the data of the selection signal stored in the LUT 63, the gate circuits 34a to 34d switch from closed to open. In this case, the opened gate circuit maintains the opened state until a

next CLK 73 for LUT (as a readout signal) is inputted.

[0101] It should be noted that a scheme may be adopted in which the CLK 73 for LUT has a predetermined pulse width and the opening and closing of the gate circuits 34a to 34d is properly operated only if the DC blocking and clipping circuit 31 determines (or judges) the predetermined pulse width and the predetermined level. With such a scheme, a malfunction caused by a noise or the like can be reduced. In this manner, the DC blocking and clipping circuit 31 may have a function to determine a CLK 73 for LUT as a readout signal.

[0102] Further, transmission signals are sent out via the transmission and reception signal line 11A to the plurality of C-MUTs 8a to 8d. Therefore, the transmission signals are applied onto the plurality of C-MUTs 8a to 8d through the opened gate circuit.

[0103] Again, after the transmission time period T_b in Fig. 11 (B), a CLK 73 for LUT is sent out at the start of the reception time period T_c , and thereby the LUT 63 selects a C-MUT as an ultrasound transducer for reception.

[0104] Examples of set patterns of C-MUTs stored in the LUT 63 of Fig. 10 and selectively used for transmission and reception are shown in tables of Figs. 12(A) and 12(B).

[0105] CLK Nos. in the tables of Figs. 12(A) and 12(B) indicate the CLKs 73 for LUT shown in Fig. 11 (B) and inputted into the LUT 63 of Fig. 10. The set pattern A in Fig. 12(A) shows the case in which each ultrasound transducer is selected and used for transmission or reception. Also in a scheme that uses the LUT 63, such setting of the set pattern A allows ultrasound transducers to be changed over one by one.

[0106] Further, the set pattern B in Fig. 12(B) shows the case in which a plurality of ultrasound transducers are used for transmission. The plurality of C-MUTs to be selected and used are registered for a same (one) CLK No., and thereby ultrasound can be transmitted by the plurality of ultrasound transducers. Further, Fig. 12(B) shows an example in which the ultrasound transducers are changed over one after another at the time of reception.

[0107] In this manner of the present embodiment, before ultrasound is actually transmitted and received, if an ultrasound transducer to be driven which is used to transmit and receive ultrasound is linked with a clock number and registered on (stored in) the LUT 63, ultrasound can be transmitted and received by one or more ultrasound transducers.

[0108] That is, in the present embodiment, as selection signals, a selection signal for transmission and a selection signal for reception that allow separately setting an ultrasound transducer selected for transmission and an ultrasound transducer selected for reception are stored in the LUT 63, so as to enable an ultrasound transducer used for transmission and an ultrasound transducer used for reception to be changed.

[0109] In addition, as shown in Fig. 12(B), a plurality

of ultrasound transducers may be selected at a time to transmit ultrasound. In this manner, a plurality of ultrasound transducers are selected at a time to transmit ultrasound, and thereby ultrasound with large signal strength can be transmitted. In this case, a reception signal with a high S/N can be obtained. Therefore, an ultrasound tomographic image with a high image quality can be displayed.

[0110] In the configuration illustrated in Fig. 10, a counter (e.g., as the OSC portion 64) that counts the number of the inputted CLKs 73 for LUT is installed in the selection circuit 62, and the number of the CLKs 73 for LUT counted by the counter may be used to identify a CLK No. shown in Fig. 12.

[0111] Then, a count value corresponding to a CLK No. from the counter may be applied to the LUT 63 as an address signal and data of a selection signal linked with the count value and stored in the LUT 63 may be read out from the LUT 63. That is, the counter may be used as a signal generating portion.

[0112] It should be noted that a method for storing a selection signal in the LUT 63 is not limited to the method shown in Fig. 11(A); data of a selection signal may also be stored in the LUT 63 by other means. For example, a data writing device such as a ROM writer may be used to write in advance a transducer selection code 71 into a ROM used as the LUT 63, and the ROM in which the transducer selection code 71 is written may be used as the LUT 63.

[0113] In addition, the foregoing example has described the case in which the two-electrode-type C-MUT 8i shown in Fig. 1 is used, but the foregoing example may be applied to the case of the three-electrode-type C-MUTs described in the second embodiment.

[0114] Fig. 13 illustrates a configuration around the signal determining portion 61 in which the third embodiment is applied to the three-electrode-type C-MUTs 48a to 48c.

[0115] The gate circuits 34a to 34c contiguous to the C-MUTs 48a to 48c are on the transmission and reception signal line 11A, and the selection circuit 62 is also connected with the gate circuits 34a to 34c.

[0116] As described above, a plurality of ultrasound transducers are selected to transmit ultrasound, and thereby comparatively large ultrasound can be emitted to an object to be examined, so that the sensitivity to receive ultrasound can be increased.

[0117] Furthermore, if a ultrasound transducer to be selected is stored in the LUT 63 as data in advance, it is not necessary to insert a long code between transmission and reception; for example, the insertion of one pulse will suffice. Thus, a time period having CLKs 73 for LUT to select a transducer can be shortened, and as a result, a frame rate in an ultrasound tomographic image for one screen (one frame) can be increased.

[0118] Additionally, as in the first embodiment, since the transmission and reception signal line 11A also functions as a selection signal line, the number of signal lines needed to be inserted into the ultrasound probe 2 can be

reduced. Therefore, for example, an outer diameter of the insertion portion can be reduced, so that advantageously, the present embodiment can be applied to wider use.

(Fourth Embodiment)

[0119] In the foregoing embodiments, the case in which C-MUTs are used as ultrasound transducers has been described. The present invention is not limited to the case in which the ultrasound transducers are C-MUTs. The present invention may also be applied to ultrasound transducers formed by using piezoelectric elements (hereinafter, referred to as the piezoelectric transducers).

[0120] An ultrasound diagnostic apparatus 1D of a fourth embodiment shown in Fig. 14 uses, for example, PZT as piezoelectric transducers.

[0121] The ultrasound diagnostic apparatus 1D illustrated in Fig. 14 includes an ultrasound probe 2D, an observing apparatus 3D, and a monitor 4. It should be noted that the ultrasound probe 2D and the observing apparatus 3D in the present embodiment have the same configurations as those in Fig. 1. Therefore, also in the present embodiment, a transmission and reception signal line 11A and a ground line connected with ground terminal are inserted into an insertion portion 5 of the ultrasound probe 2D. In the present embodiment, a power supply line 86A is inserted into the insertion portion 5 as described later.

[0122] In the ultrasound probe 2D, lead zirconate titanate (abbreviated as PZT) 78i is used as piezoelectric elements instead of the C-MUT 48i in the ultrasound probe 2B shown in Fig. 7.

[0123] One electrode 81i of each PZT 78i constituting the ultrasound transducer array 10D is connected with one end of a signal determining portion 79i via a signal line 83i, and the other end of the signal determining portion 79i is connected with the common transmission and reception signal line 11A.

[0124] The other electrode 82i of the PZT 81i is connected with the ground via a signal line 84i.

[0125] Further, because the observing apparatus 3D does not need a DC bias in the observing apparatus 3B shown in Fig. 7, the DC bias outputting portion 12 is removed and a power supply circuit 85 is included.

[0126] That is, the observing apparatus 3D includes a transmitting portion 14 and a receiving portion 15 connected with one end of the transmission and reception signal line 11B, the other end of which is connected with a transmission and reception signal line 11A, a control portion 18 that controls the transmitting portion 14 and the receiving portion 15, and an operation portion 19.

[0127] Further, a power supply line 86B in the observing apparatus 3D is connected with one end of the ultrasound probe 1D and the power supply circuit 85 supplies power supply (power) for operation to the signal determining portion 79i, with which the other end of the power

supply line 86A is connected. The configuration of the signal determining portion 79i is similar to that in Fig. 9. However, the signal determining portion 79i is supplied with the power supply for operation via the power supply line 86A.

[0128] The others are similar to those shown in Fig. 7. An operation of the present embodiment is as follows.

[0129] The transmission signal outputting portion 16 outputs a transmission signal, and the signal mixing portion (signal superimposing portion) 17 mixes the transmission signal with a selection signal and transmits the signal to the signal determining portion 79i via the transmission and reception signal line 11A.

[0130] Each signal determining portion 79i determines by the selection signal whether or not the transmission signal is for a PZT 78i selected by the selection signal, and if it is determined that the transmission signal is for the selected PZT 78i, the transmission signal is applied onto the PZT 78i.

[0131] Then, the PZT 78i transmits ultrasound. The transmitted ultrasound is reflected from a part in which acoustic impedance is changed, received by the PZT 78i used for the transmission, and converted into an ultrasound signal.

[0132] The ultrasound signal passes through the signal determining portion 79i and the transmission and reception signal lines 11A and 11B, and is amplified by the amplifier portion 25. Then, the amplified signal is imaged at the reception signal processing portion 26 and displayed on the monitor 4.

[0133] The power for the signal determining portion 79i is supplied from the power supply circuit 85 via the power supply lines 86B and 86A.

[0134] Fig. 15 illustrates an example of a configuration of, for example, three PZTs 78a to 78c and signal determining portions 79a to 79c. The signal determining portions 79a to 79c are connected with the PZTs 78a to 78c, respectively, and the signal determining portions 79a to 79c are connected with the common transmission and reception signal line 11A.

[0135] Besides the transmission and reception signal line 11A, the power supply line 86A is provided to operate the signal determining portions 79a to 79c. A configuration of the signal determining portion 79i is identical to the three-electrode-type configuration shown in Fig. 9, and because the present embodiment does not need the supply of a DC bias, a selection signal is taken out of a transmission signal by a clipping circuit (51i, if denoted by the same reference numeral in Fig. 9).

[0136] As in the first embodiment, also in the present embodiment, a transducer can be selected by the signal determining portion 79i with the transmission and reception signal line 11A also functioning as a selection signal line. Therefore, the number of signal lines needed to be inserted into the ultrasound probe 2D can be reduced. In addition, for example, an outer diameter of the insertion portion can be reduced, so that advantageously, the present embodiment can be applied to wider use.

[0137] Further, the transducer selection circuit scheme using the LUT 63 and being shown in Fig. 10 and Fig. 11 can be applied as selecting means in which piezoelectric transducers are used.

[0138] In all the above-described embodiments, as means for selecting a transducer, pulse counting has been used, but as other means, a cycle and the number of a sinusoidal signal may be changed and judged. Also, in place of the gate circuit, for example, a semiconductor switch or other switches that can be switched on/off by a control signal may also be used.

Claims

1. An ultrasound diagnostic apparatus (1) comprising:

a plurality of ultrasound transducers (8a, 8b, 8n);
a transmission signal outputting portion (16) configured to generate transmission signals for driving the plurality of ultrasound transducers;
transmission and reception signal lines (11A, 11B) that send transmission and reception signals for transmitting and receiving ultrasound to the plurality of ultrasound transducers; and
a direct current blocking circuit (31) configured to block a direct current bias component sent through the transmission and reception signal lines, **characterized in that**

the transmission and reception signal lines send the transmission signal with a selection signal for selecting an ultrasound transducer to be driven out of the plurality of ultrasound transducers, and

the apparatus further comprises:

signal determining portions (9a, 9b, 9n) provided close to the plurality of ultrasound transducers and configured to:

make a determination based on the selection signal, the selection signal being sent out in synchronization with the transmission signal for forming the transmission and reception signal, and electrically couple the ultrasound transducer to be driven with the transmission and reception signal line in accordance with a result of the determination;

a signal mixing portion (17) configured to superimpose the transmission signal with the selection signal;

a control portion (18) configured to control a superimposing timing of the transmission signal with the selection signal; and
a direct current bias outputting portion (12) configured to superimpose a direct current

bias on the transmission signal on which the selection signal is superimposed, wherein the direct current blocking circuit is provided in each of the signal determining portions and is further configured to:

block a direct current bias component superimposed on the transmission and reception signal, and
separate and extract the selection signal on the transmission and reception signal line, the selection signal being superimposed at a position before a signal waveform of the transmission signal.

2. The ultrasound diagnostic apparatus according to claim 1, wherein

the signal determining portion further includes a pulse counter (32i) configured to count a number of pulses forming the selection signal, and the signal determining portion is further configured to determine the ultrasound transducer to be driven in accordance with the number of the pulses counted by the pulse counter.

3. The ultrasound diagnostic apparatus according to claim 1, wherein the signal determining portion further includes:

a pulse counter (32i) configured to count a number of pulses forming the selection signal;
a judging portion (33i) configured to judge the ultrasound transducer to be driven according to the number of the pulses counted by the pulse counter; and
a gate circuit (34i) configured to open and close for applying the transmission signal onto the ultrasound transducer to be driven.

4. The ultrasound diagnostic apparatus according to claim 3, wherein

the gate circuit is configured to switch from closed to open so as to apply the transmission signal to the ultrasound transducer to be driven in response to a control signal from the judgement of the judging portion.

5. The ultrasound diagnostic apparatus according to claim 1, wherein

the plurality of ultrasound transducers are formed with capacitive ultrasound transducers.

6. The ultrasound diagnostic apparatus according to claim 1, wherein

the plurality of ultrasound transducers and the signal determining portions are provided at a distal end portion (10) of an elongate insertion portion (5), and the

transmission and reception signal line inserted into the insertion portion is, via a connector, detachably connected with an observing apparatus (3) including a transmitting portion (14) that comprises the transmission signal outputting portion and the signal mixing portion, and a receiving portion (15) configured to perform signal processing on a reception signal received by the plurality of ultrasound transducers.

7. The ultrasound diagnostic apparatus according to claim 6, wherein the observing apparatus includes the signal mixing portion as a signal superimposing portion (17) configured to superimpose the selection signal on the transmission signal and before the signal waveform of the transmission signal.
8. The ultrasound diagnostic apparatus according to claim 1, wherein the signal determining portion includes a voltage converting circuit (35) configured to convert a direct current bias component superimposed on the transmission signal and sent, into a predetermined power supply voltage for operating the signal determining portion.
9. An ultrasound diagnostic apparatus comprising:
 - a plurality of ultrasound transducers (8a, 8b, 8n);
 - a transmission signal outputting portion (16) configured to generate transmission signals for driving the plurality of ultrasound transducers; transmission and reception signal lines (11A, 11B) that send transmission and reception signals for transmitting and receiving ultrasound to the plurality of ultrasound transducers; and
 - a direct current blocking circuit (31) configured to block a direct current bias component sent through the transmission and reception signal lines, **characterized in that** the transmission and reception signal lines send the transmission signal with a readout signal for reading out a selection signal for selecting an ultrasound transducer to be driven out of the plurality of ultrasound transducers, and the apparatus further comprises:

a selection circuit (62) provided close to the plurality of ultrasound transducers and configured to:

make a determination based on the readout signal, the readout signal being sent out in synchronization with the transmission signal for forming the transmission and reception signal, and electrically couple the ultrasound transducer to be driven with the transmission

and reception signal line in accordance with a result of the determination, the selection circuit comprising:

the direct current blocking circuit; a selection look-up table portion (63) in which the selection signal is stored in advance; a signal generating portion configured to generate a signal for reading out data of the selection signal from the selection look-up table portion in response to an application of the readout signal; and a gate circuit (34a, 34b, 34c, 34d) configured to open and close for applying the transmission signal onto the ultrasound transducer to be driven;

a signal mixing portion (17) configured to superimpose the transmission signal with the readout signal; a control portion (18) configured to control a superimposing timing of the transmission signal with the readout signal; and a direct current bias outputting portion (12) configured to superimpose a direct current bias on the transmission signal on which the readout signal is superimposed, wherein the direct current blocking circuit is provided in the selection circuit and is further configured to:

block a direct current bias component superimposed on the transmission and reception signal, and separate and extract the readout signal on the transmission and reception signal line, the readout signal being superimposed at a position before a signal waveform of the transmission signal.

10. The ultrasound diagnostic apparatus according to claim 9, wherein the selection look-up table portion is configured to store, as the selection signals, a selection signal for transmission and a selection signal for reception that allow separately setting an ultrasound transducer selected for transmission and an ultrasound transducer selected for reception to enable an ultrasound transducer used for transmission and an ultrasound transducer used for reception to be changed.
11. The ultrasound diagnostic apparatus according to

claim 9, wherein
the plurality of ultrasound transducers are formed
with capacitive ultrasound transducers.

12. The ultrasound diagnostic apparatus according to claim 9, wherein
the selection circuit includes a data storage portion (63) configured to store selection signal data for, in case of superimposing the readout signal before the signal waveform of the transmission signal to be sent via the transmission and reception signal line, selecting the ultrasound transducer to be driven corresponding to the readout signal. 5 10
13. The ultrasound diagnostic apparatus according to claim 9, wherein
the plurality of ultrasound transducers and the selection circuit are provided at a distal end portion (10) of an elongate insertion portion (5), and the transmission and reception signal line inserted into the insertion portion is, via a connector, detachably connected with an observing apparatus (3) including a transmitting portion (14) that comprises the transmission signal outputting portion and the signal mixing portion, and a receiving portion (15) configured to perform signal processing on a reception signal received by the plurality of ultrasound transducers. 15 20 25
14. The ultrasound diagnostic apparatus according to claim 13, wherein the observing apparatus includes the signal mixing portion as a signal superimposing portion (17) configured to superimpose the readout signal on the transmission signal and before the signal waveform of the transmission signal. 30 35
15. The ultrasound diagnostic apparatus according to claim 12, wherein
the data storage portion is configured to store the selection signal data that allows selecting one or more ultrasound transducers as an ultrasound transducer to be driven corresponding to a single pulse for forming the readout signal. 40
16. The ultrasound diagnostic apparatus according to claim 9, further comprising a signal determining portion including a voltage converting circuit (35) configured to convert a direct current bias component superimposed on the transmission signal and sent, into a predetermined power supply voltage for operating the signal determining portion. 45 50

Patentansprüche

1. Ultraschall Diagnosevorrichtung (1), die umfasst:
eine Vielzahl von Ultraschallwandlern (8a, 8b, 8n); 55

eine Übertragungssignalausgabeeinheit (16), die dazu eingerichtet ist, Übertragungssignale zum Ansteuern der Vielzahl von Ultraschallwandlern zu erzeugen;
Übertragungssignal- und Empfangssignalleitungen (11A, 11B), die Übertragungs- und Empfangssignale senden, um Ultraschall zu der Vielzahl von Ultraschallwandlern zu übertragen und von dieser zu empfangen; und
einen Gleichstromsperrkreis (31), der dazu eingerichtet ist, eine über die Übertragungssignal- und Empfangssignalleitungen gesendete Gleichstromvorspannungskomponente zu sperren, **dadurch gekennzeichnet, dass**
die Übertragungssignal- und Empfangssignalleitungen das Übertragungssignal mit einem Auswahlsignal senden, zum Auswählen eines anzusteuern Ultraschallwandlers aus der Vielzahl von Ultraschallwandlern, und
die Vorrichtung des Weiteren umfasst:

Signalbestimmungseinheiten (9a, 9b, 9n), die in der Nähe der Vielzahl von Ultraschallwandlern angeordnet sind und dazu eingerichtet sind:

eine Bestimmung basierend auf dem Auswahlsignal auszuführen, wobei das Auswahlsignal synchron mit dem Übertragungssignal ausgesendet wird, um das Übertragungs- und Empfangssignal zu bilden, und
den anzusteuern Ultraschallwandler anhand des Ergebnisses der Bestimmung elektrisch mit der Übertragungssignal- und Empfangssignalleitung zu koppeln;
eine Signalmischeinheit (17), die dazu eingerichtet ist, das Übertragungssignal mit dem Auswahlsignal zu überlagern;
eine Steuerungseinheit (18), die dazu eingerichtet ist, einen Überlagerungszeitpunkt des Übertragungssignals mit dem Auswahlsignal zu steuern; und
eine Gleichstromvorspannungsausgabeeinheit (12), die dazu eingerichtet ist, eine Gleichstromvorspannung dem Übertragungssignal zu überlagern, dem das Auswahlsignal überlagert ist, wobei der Gleichstromsperrkreis in jeder der Signalbestimmungseinheiten vorgesehen ist und des Weiteren dazu eingerichtet ist:

eine Gleichstromvorspannungskomponente zu sperren, die dem Übertragungs- und Empfangssig-

- nal überlagert ist, und das Auswahlsignal aus der Übertragungssignal- und Empfangssignalleitung zu separieren und extrahieren, wobei das Auswahlsignal an einer Position vor einer Signalwellenform des Übertragungssignals überlagert wird. 5
2. Ultraschall Diagnosevorrichtung nach Anspruch 1, wobei die Signalbestimmungseinheit des Weiteren einen Pulszähler (32i) umfasst, der dazu eingerichtet ist, eine Anzahl an Impulsen zu zählen, die das Auswahlsignal bilden, und die Signalbestimmungseinheit des Weiteren dazu eingerichtet ist, den anzusteuern den Ultraschallwandler anhand der Anzahl an Impulsen zu bestimmen, die von dem Impulszähler gezählt worden sind. 10
3. Ultraschall Diagnosevorrichtung nach Anspruch 1, wobei die Signalbestimmungseinheit des Weiteren umfasst: 20
- einen Impulszähler (32i), der dazu eingerichtet ist, eine Anzahl an Impulsen zu zählen, die das Auswahlsignal bilden; 25
- eine Beurteilungseinheit (33i), die dazu eingerichtet ist, den anzusteuern den Ultraschallwandler anhand der Anzahl an Impulsen zu beurteilen, die von dem Impulszähler gezählt worden sind; und 30
- eine Torschaltung (34i), die dazu eingerichtet ist, zu öffnen und zu schließen, um das Übertragungssignal an den anzusteuern den Ultraschallwandler anzulegen. 35
4. Ultraschall Diagnosevorrichtung nach Anspruch 3, wobei die Torschaltung dazu eingerichtet ist, von geschlossen auf geöffnet zu schalten, um das Übertragungssignal an den anzusteuern den Ultraschallwandler anzulegen, als Reaktion auf ein Steuerungssignal von der Beurteilung der Beurteilungseinheit. 40
5. Ultraschall Diagnosevorrichtung nach Anspruch 1, wobei die Vielzahl von Ultraschallwandlern mit kapazitiven Ultraschallwandlern ausgebildet sind. 45
6. Ultraschall Diagnosevorrichtung nach Anspruch 1, wobei die Vielzahl von Ultraschallwandlern und die Signalbestimmungseinheiten in einem äußeren Endabschnitt (10) einer länglichen Einbringungseinheit (5) angeordnet sind, und die in die Einbringungseinheit eingebrachte Übertragungssignal- und Empfangssignalleitung über einen Anschluss lösbar mit einer Überwachungs Vorrichtung (3) verbunden ist, die umfasst: eine Übertragungseinheit (14), die die Übertragungssignalausgabereinheit und die Signal- 50
- mischeinheit umfasst, und eine Empfangseinheit (15), die dazu eingerichtet ist, eine Signalverarbeitung eines Empfangssignals auszuführen, das von der Vielzahl von Ultraschallwandlern empfangen worden ist.
7. Ultraschall Diagnosevorrichtung nach Anspruch 6, wobei die Überwachungs Vorrichtung die Signalmischeinheit in Form einer Signalüberlagerungseinheit (17) umfasst, die dazu eingerichtet ist, das Übertragungssignal vor der Signalwellenform des Übertragungssignals mit dem Auswahlsignal zu überlagern.
8. Ultraschall Diagnosevorrichtung nach Anspruch 1, wobei die Signalbestimmungseinheit einen Spannungswandlerkreis (35) aufweist, der dazu eingerichtet ist, eine Gleichstromvorspannungskomponente, die dem Übertragungssignal überlagert und gesendet worden ist, in eine vorbestimmte Energieversorgungsspannung zum Ausführen der Signalbestimmungseinheit umzuwandeln.
9. Ultraschall Diagnosevorrichtung, die umfasst: 25
- eine Vielzahl von Ultraschallwandlern (8a, 8b, 8n);
- eine Übertragungssignalausgabereinheit (16), die dazu eingerichtet ist, Übertragungssignale zum Ansteuern der Vielzahl von Ultraschallwandlern zu erzeugen; Übertragungssignal- und Empfangssignalleitungen (11A, 11B), die Übertragungs- und Empfangssignale senden, um Ultraschall zu der Vielzahl von Ultraschallwandlern zu übertragen und von dieser zu empfangen; und
- einen Gleichstromsperrkreis (31), der dazu eingerichtet ist, eine Gleichstromvorspannungskomponente zu sperren, die über die Übertragungssignal- und Empfangssignalleitungen gesendet worden ist, **dadurch gekennzeichnet, dass**
- die Übertragungssignal- und Empfangssignalleitungen das Übertragungssignal mit einem Auslesesignal zum Auslesen eines Auswahlsignals senden, um einen anzusteuern den Ultraschallwandler aus der Vielzahl von Ultraschallwandlern auszuwählen, und die Vorrichtung des Weiteren umfasst:
- einen Auswahlstromkreis (62), der in der Nähe der Vielzahl von Ultraschallwandlern angeordnet ist und dazu eingerichtet ist:
- eine Bestimmung basierend auf dem Auslesesignal auszuführen, wobei das Auslesesignal synchron mit dem Übertragungssignal ausgesendet wird, um

das Übertragungs- und Empfangssignal zu bilden, und
den anzusteuern den Ultraschallwandler anhand des Ergebnisses der Bestimmung elektrisch mit der Übertragungssignal- und Empfangssignalleitung zu koppeln, wobei der Auswahlstromkreis umfasst:

den Gleichstromsperrkreis;
eine Auswahlnachschlagetableneinheit (63), in der das Auswahlsignal im Voraus gespeichert ist;
eine Signalerzeugungseinheit, die dazu eingerichtet ist, ein Signal zum Auslesen von Daten des Auswahlsignals aus der Auswahlnachschlagetableneinheit zu erzeugen, als Reaktion auf ein Verwenden des Auslesesignals; und
eine Torschaltung (34a, 34b, 34c, 34d), die dazu eingerichtet ist, zu öffnen und zu schließen, um das Übertragungssignal an den anzusteuern den Ultraschallwandler anzulegen;
eine Signalmischeinheit (17), die dazu eingerichtet ist, das Übertragungssignal dem Auslesesignal zu überlagern;
eine Steuerungseinheit (18), die dazu eingerichtet ist, einen Überlagerungszeitpunkt des Übertragungssignals mit dem Auslesesignal zu steuern; und
eine Gleichstromvorspannungsausgabereinheit (12), die dazu eingerichtet ist, eine Gleichstromvorspannung über das Übertragungssignal zu überlagern, über das das Auslesesignal überlagert ist, wobei der Gleichstromsperrkreis in dem Auswahlstromkreis angeordnet ist und des Weiteren dazu eingerichtet ist:

eine Gleichstromvorspannungskomponente zu sperren, die dem Übertragungs- und Empfangssignal überlagert ist, und
das Auslesesignal aus der Übertragungssignal- und Empfangssignalleitung zu separieren und extrahieren, wobei das Auslesesignal an einer Position vor einer Signalwellenform des Übertragungssig-

nals überlagert wird.

10. Ultraschalldiagnosevorrichtung nach Anspruch 9, wobei
die Auswahlnachschlagetableneinheit dazu eingerichtet ist, ein Auswahlsignal zum Übertragen und ein Auswahlsignal zum Empfangen als die Auswahlsignale zu speichern, die es ermöglichen, einen zum Übertragen ausgewählten Ultraschallwandler und einen zum Empfangen ausgewählten Ultraschallwandler getrennt voneinander zu bestimmen, so dass ein zum Übertragen verwendeter Ultraschallwandler und ein zum Empfangen verwendeter Ultraschallwandler änderbar sind.
11. Ultraschalldiagnosevorrichtung nach Anspruch 9, wobei
die Vielzahl von Ultraschallwandlern mit kapazitiven Ultraschallwandlern ausgebildet sind.
12. Ultraschalldiagnosevorrichtung nach Anspruch 9, wobei
der Auswahlstromkreis eine Datenspeichereinheit (63) umfasst, die dazu eingerichtet ist, Auswahlsignaldaten zu speichern, um den anzusteuern den Ultraschallwandler anhand des Auslesesignals auszuwählen, wenn das Auslesesignal vor der Signalwellenform des Übertragungssignals überlagert wird, das über die Übertragungssignal- und Empfangssignalleitung gesendet wird.
13. Ultraschalldiagnosevorrichtung nach Anspruch 9, wobei
die Vielzahl von Ultraschallwandlern und der Auswahlstromkreis an einem äußeren Endabschnitt (10) einer länglichen Einbringungseinheit (5) vorgesehen sind, und die in die Einbringungseinheit eingebrachte Übertragungssignal- und Empfangssignalleitung über einen Anschluss lösbar mit einer Überwachungsvorrichtung (3) verbunden ist, die umfasst:
eine Übertragungseinheit (14), die die Übertragungssignalausgabereinheit und die Signalmischeinheit umfasst, und eine Empfangseinheit (15), der dazu eingerichtet ist, eine Signalverarbeitung eines Empfangssignals auszuführen, das von der Vielzahl von Ultraschallwandlern empfangen worden ist.
14. Ultraschalldiagnosevorrichtung nach Anspruch 13, wobei die Überwachungsvorrichtung die Signalmischeinheit in Form einer Signalüberlagerungseinheit (17) umfasst, die dazu eingerichtet ist, das Auslesesignal vor der Signalwellenform des Übertragungssignals über das Übertragungssignal zu überlagern.
15. Ultraschalldiagnosevorrichtung nach Anspruch 12, wobei die Datenspeichereinheit dazu einge-

richtet ist, die Auswahl signaldaten zu speichern, die die Auswahl eines oder mehrerer Ultraschallwandler als einen anzusteuern Ultraschallwandler anhand eines einfachen Impulses ermöglicht, der das Auslesesignal bildet.

16. Ultraschall Diagnosevorrichtung nach Anspruch 9, die des Weiteren eine Signalbestimmungseinheit umfasst, die einen Spannungswandlerring (35) aufweist, der dazu eingerichtet ist, eine über das Übertragungssignal überlagerte und gesendete Gleichstromvorspannungskomponente in eine vorbestimmte Energieversorgungsspannung zum Ausführen der Signalbestimmungseinheit umzuwandeln.

Revendications

1. Appareil (1) de diagnostic à ultrasons comprenant :

une pluralité de transducteurs ultrasonores (8a, 8b, 8n) ;
 une partie (16) de sortie de signaux de transmission configurée pour générer des signaux de transmission destinés à entraîner la pluralité de transducteurs ultrasonores ;
 des lignes (11A, 11B) de signaux de transmission et de réception qui envoient des signaux de transmission et de réception destinés à transmettre et à recevoir des ultrasons vers la pluralité de transducteurs ultrasonores ; et
 un circuit (31) de blocage de courant continu configuré pour bloquer une composante de polarisation continue envoyée par l'intermédiaire des lignes de signaux de transmission et de réception, **caractérisé en ce que**
 les lignes de signaux de transmission et de réception envoient les signaux de transmission avec un signal de sélection destiné à sélectionner un transducteur ultrasonore destiné à être entraîné parmi la pluralité de transducteurs ultrasonores, et l'appareil comprend en outre :

des parties (9a, 9b, 9n) de détermination de signaux prévues près de la pluralité de transducteurs ultrasonores et configurées pour :

effectuer une détermination sur la base du signal de sélection, le signal de sélection étant envoyé en synchronisation avec le signal de transmission pour former les signaux de transmission et de réception, et
 coupler électriquement le transducteur ultrasonore destiné à être entraîné avec la ligne de signaux de transmis-

sion et de réception conformément à un résultat de la détermination ;

une partie (17) de mélange de signaux configurée pour superposer le signal de transmission et le signal de sélection ;
 une partie (18) de commande configurée pour commander un cadencement de superposition du signal de transmission et du signal de sélection ; et
 une partie (12) de sortie de polarisation continue configurée pour superposer une polarisation continue sur le signal de transmission sur lequel le signal de sélection est superposé, dans lequel le circuit de blocage de courant continu est prévu dans chacune des parties de détermination de signaux et est en outre configuré pour :

bloquer une composante de polarisation continue superposée sur les signaux de transmission et de réception, et
 séparer et extraire le signal de sélection sur la ligne de signaux de transmission et de réception, le signal de sélection étant superposé au niveau d'une position avant une forme d'onde de signal du signal de transmission.

2. Appareil de diagnostic à ultrasons selon la revendication 1, dans lequel

la partie de détermination de signaux comprend en outre un compteur d'impulsions (32i) configuré pour compter un nombre d'impulsions formant le signal de sélection, et

la partie de détermination de signaux est en outre configurée pour déterminer le transducteur ultrasonore destiné à être entraîné conformément au nombre d'impulsions comptées par le compteur d'impulsions.

3. Appareil de diagnostic à ultrasons selon la revendication 1, dans lequel la partie de détermination de signaux comprend en outre :

un compteur d'impulsions (32i) configuré pour compter un nombre d'impulsions formant le signal de sélection ;

une partie de jugement (33i) configurée pour juger le transducteur ultrasonore destiné à être entraîné conformément au nombre d'impulsions comptées par le compteur d'impulsions ; et

un circuit de porte (34i) configuré pour s'ouvrir et se fermer pour appliquer le signal de transmission sur le transducteur ultrasonore destiné à être entraîné.

4. Appareil de diagnostic à ultrasons selon la revendication 3, dans lequel
le circuit de porte est configuré pour commuter de l'état fermé à l'état ouvert de façon à appliquer le signal de transmission au transducteur ultrasonore destiné à être entraîné en réponse à un signal de commande provenant du jugement de la partie de jugement. 5
5. Appareil de diagnostic à ultrasons selon la revendication 1, dans lequel
la pluralité des transducteurs ultrasonores sont formés avec des transducteurs ultrasonores capacitifs. 10
6. Appareil de diagnostic à ultrasons selon la revendication 1, dans lequel
la pluralité de transducteurs ultrasonores et les parties de détermination de signaux sont prévus au niveau d'une partie d'extrémité distale (10) d'une partie d'insertion allongée (5), et la ligne de signaux de transmission et de réception insérée dans la partie d'insertion est, via un connecteur, connectée de manière détachable à un appareil d'observation (3) incluant une partie de transmission (14) qui comprend la partie de sortie de signaux de transmission et la partie de mélange de signaux, et une partie de réception (15) configurée pour réaliser un traitement de signal sur un signal de réception reçu par la pluralité de transducteurs ultrasonores. 15 20 25 30
7. Appareil de diagnostic à ultrasons selon la revendication 6, dans lequel
l'appareil d'observation comprend une partie de mélange de signaux en tant que partie (17) de superposition de signaux configurée pour superposer le signal de sélection sur le signal de transmission et avant la forme d'onde de signal du signal de transmission. 35
8. Appareil de diagnostic à ultrasons selon la revendication 1, dans lequel
la partie de détermination de signaux comprend un circuit (35) de conversion de tension configuré pour convertir une composante de polarisation continue superposée sur le signal de transmission et envoyée, en une tension d'alimentation prédéterminée destinée à actionner la partie de détermination de signaux. 40 45
9. Appareil de diagnostic à ultrasons comprenant : 50
 - une pluralité de transducteurs ultrasonores (8a, 8b, 8n) ;
 - une partie (16) de sortie de signaux de transmission configurée pour générer des signaux de transmission destinés à entraîner la pluralité de transducteurs ultrasonores ;
 - des lignes (11A, 11B) de signaux de transmis-

sion et de réception qui envoient des signaux de transmission et de réception destinés à transmettre et à recevoir des ultrasons vers la pluralité de transducteurs ultrasonores ; et
un circuit (31) de blocage de courant continu configuré pour bloquer une composante de polarisation continue envoyée par l'intermédiaire des lignes de signaux de transmission et de réception, **caractérisé en ce que**
les lignes de signaux de transmission et de réception envoient les signaux de transmission avec un signal d'extraction destiné à extraire un signal de sélection destiné à sélectionner un transducteur ultrasonore devant être entraîné parmi la pluralité de transducteurs ultrasonores, et
l'appareil comprend en outre :

un circuit de sélection (62) prévu près de la pluralité de transducteurs ultrasonores et configuré pour :

effectuer une détermination sur la base du signal d'extraction, le signal d'extraction étant envoyé en synchronisation avec le signal de transmission pour former les signaux de transmission et de réception, et
coupler électriquement le transducteur ultrasonore destiné à être entraîné avec la ligne de signaux de transmission et de réception conformément à un résultat de la détermination, le circuit de sélection comprenant :

le circuit de blocage de courant continu ;
une partie (63) de table de consultation de sélection dans laquelle le signal de sélection est mémorisé à l'avance ;
une partie de génération de signal configurée pour générer un signal destiné à extraire des données du signal de sélection à partir de la partie de table de consultation de sélection en réponse à une application du signal d'extraction ; et
un circuit de porte (34a, 34b, 34c, 34d) configuré pour s'ouvrir et se fermer pour appliquer le signal de transmission sur le transducteur

ultrasonore destiné à être entraîné ;

une partie (17) de mélange de signaux configurée pour superposer le signal de transmission et le signal d'extraction ;

- une partie (18) de commande configurée pour commander un cadencement de superposition du signal de transmission et du signal d'extraction ; et
- une partie (12) de sortie de polarisation continue configurée pour superposer une polarisation continue sur le signal de transmission sur lequel le signal d'extraction est superposé,
- dans lequel le circuit de blocage de courant continu est prévu dans le circuit de sélection et est en outre configuré pour :
- bloquer une composante de polarisation continue superposée sur les signaux de transmission et de réception, et
 - séparer et extraire le signal d'extraction sur la ligne de signaux de transmission et de réception, le signal d'extraction étant superposé au niveau d'une position avant une forme d'onde de signal du signal de transmission.
- 10.** Appareil de diagnostic à ultrasons selon la revendication 9, dans lequel
- la partie de table de consultation de sélection est configurée pour mémoriser, en tant que signaux de sélection, un signal de sélection pour la transmission et un signal de sélection pour la réception qui permettent d'établir séparément un transducteur ultrasonore sélectionné pour la transmission et un transducteur ultrasonore sélectionné pour la réception pour permettre qu'un transducteur ultrasonore utilisé pour la transmission et qu'un transducteur ultrasonore utilisé pour la réception soient changés.
- 11.** Appareil de diagnostic à ultrasons selon la revendication 9, dans lequel
- la pluralité des transducteurs ultrasonores sont formés avec des transducteurs ultrasonores capacitifs.
- 12.** Appareil de diagnostic à ultrasons selon la revendication 9, dans lequel
- le circuit de sélection comprend une partie (63) de stockage de données configurée pour stocker des données de signaux de sélection pour, dans le cas d'une superposition du signal d'extraction avant la forme d'onde de signal du signal de transmission destiné à être envoyé via la ligne de signaux de transmission et de réception, sélectionner le transducteur ultrasonore destiné à être entraîné correspondant au signal d'extraction.
- 13.** Appareil de diagnostic à ultrasons selon la revendication 9, dans lequel
- la pluralité de transducteurs ultrasonores et le circuit de sélection sont prévus au niveau d'une partie d'ex-
- trémité distale (10) d'une partie d'insertion allongée (5), et la ligne de signaux de transmission et de réception insérée dans la partie d'insertion est, via un connecteur, connectée de manière détachable à un appareil d'observation (3) comprenant une partie de transmission (14) qui comprend une partie de sortie de signaux de transmission et la partie de mélange de signaux, et une partie de réception (15) configurée pour réaliser un traitement de signal sur un signal de réception reçu par la pluralité de transducteurs ultrasonores.
- 14.** Appareil de diagnostic à ultrasons selon la revendication 13, dans lequel l'appareil d'observation comprend la partie de mélange de signaux en tant que partie (17) de superposition de signaux configurée pour superposer le signal d'extraction sur le signal de transmission et avant la forme d'onde de signal du signal de transmission.
- 15.** Appareil de diagnostic à ultrasons selon la revendication 12, dans lequel
- la partie de stockage de données est configurée pour stocker les données de signaux de sélection qui permettent la sélection d'un ou de plusieurs transducteurs ultrasonores en tant que transducteur ultrasonore destiné à être entraîné correspondant à une impulsion unique pour former le signal d'extraction.
- 16.** Appareil de diagnostic à ultrasons selon la revendication 9, comprenant en outre une partie de détermination de signaux comprenant un circuit de conversion de tension (35) configuré pour convertir une composante de polarisation continue superposée sur le signal de transmission et envoyée, en une tension d'alimentation prédéterminée destinée à actionner la partie de détermination de signaux.

FIG.1

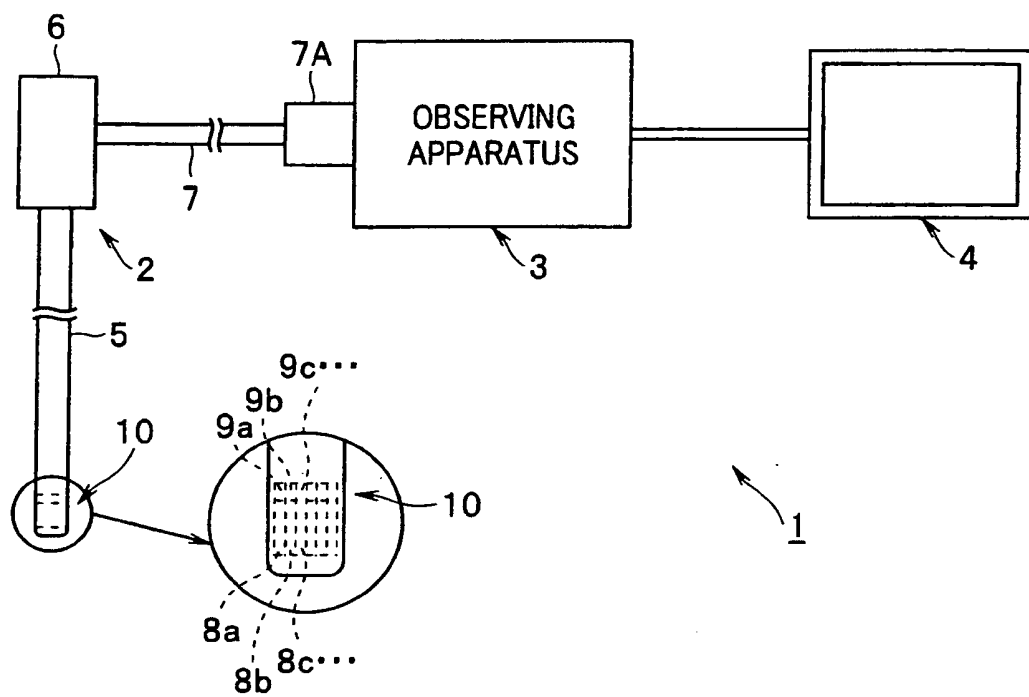


FIG.2

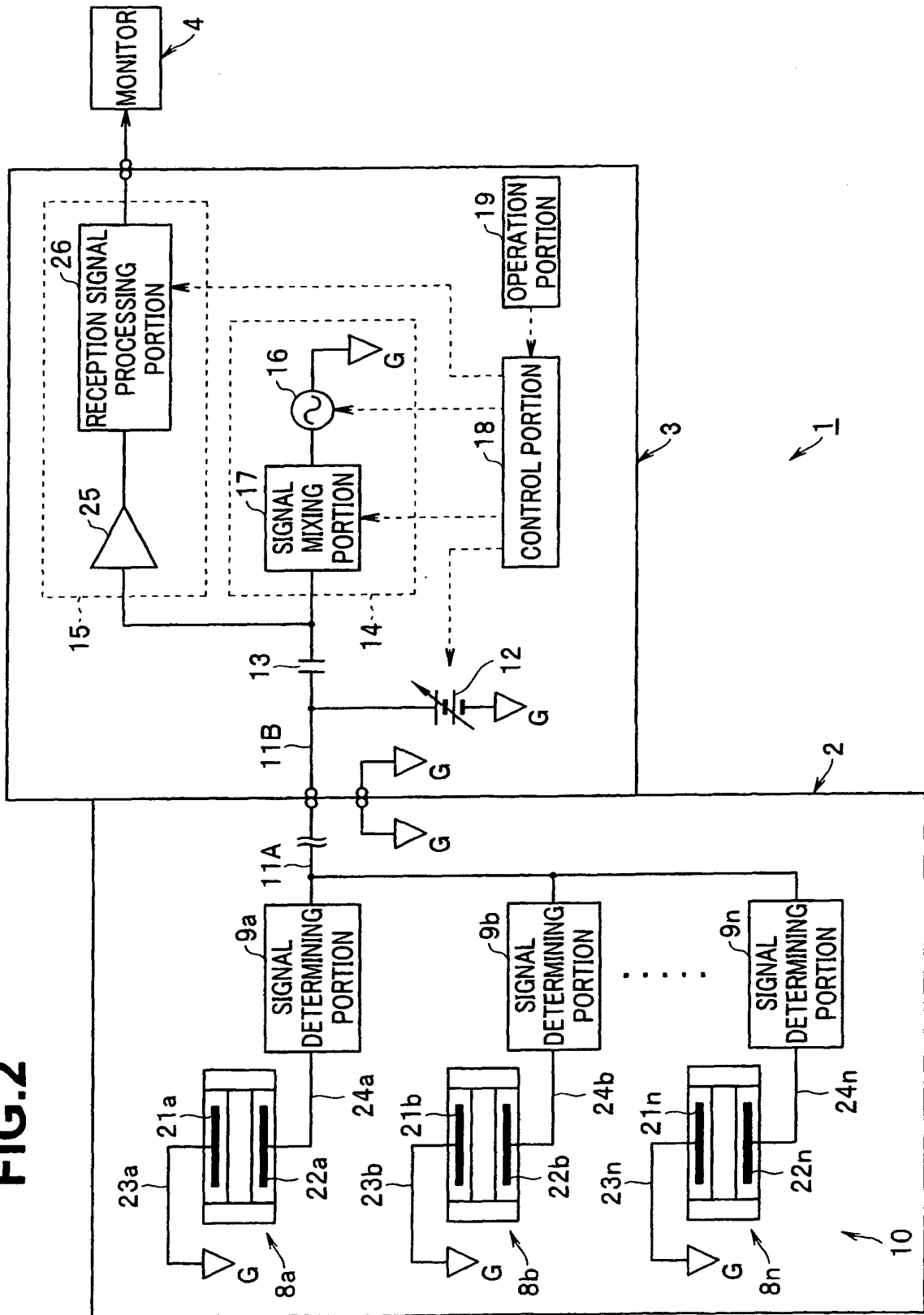


FIG.3

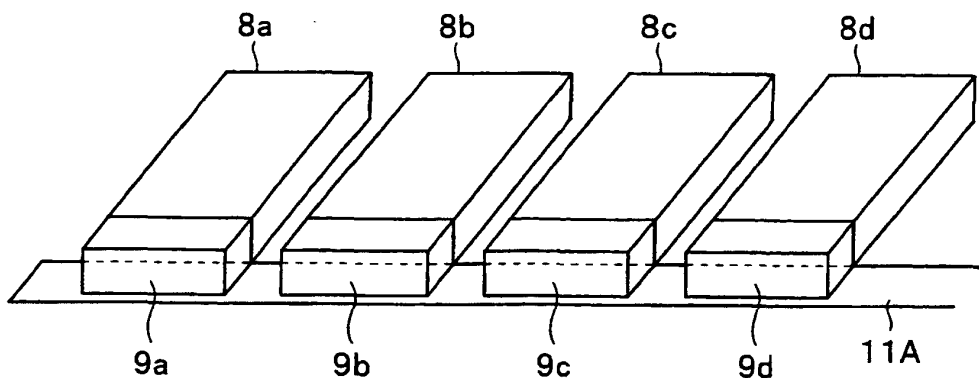


FIG.4

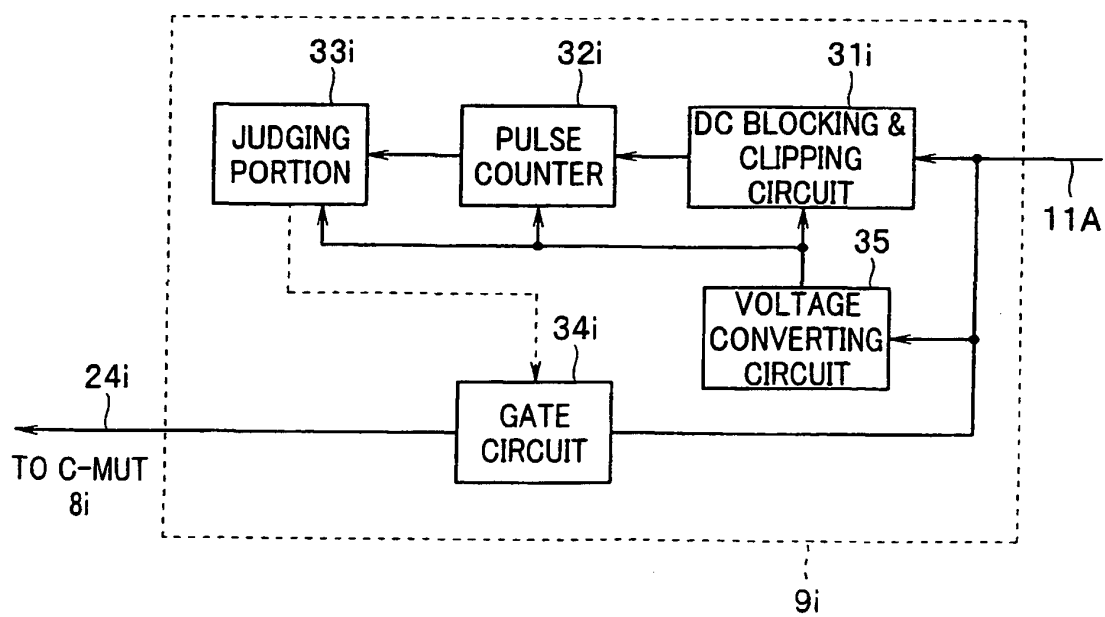


FIG.5

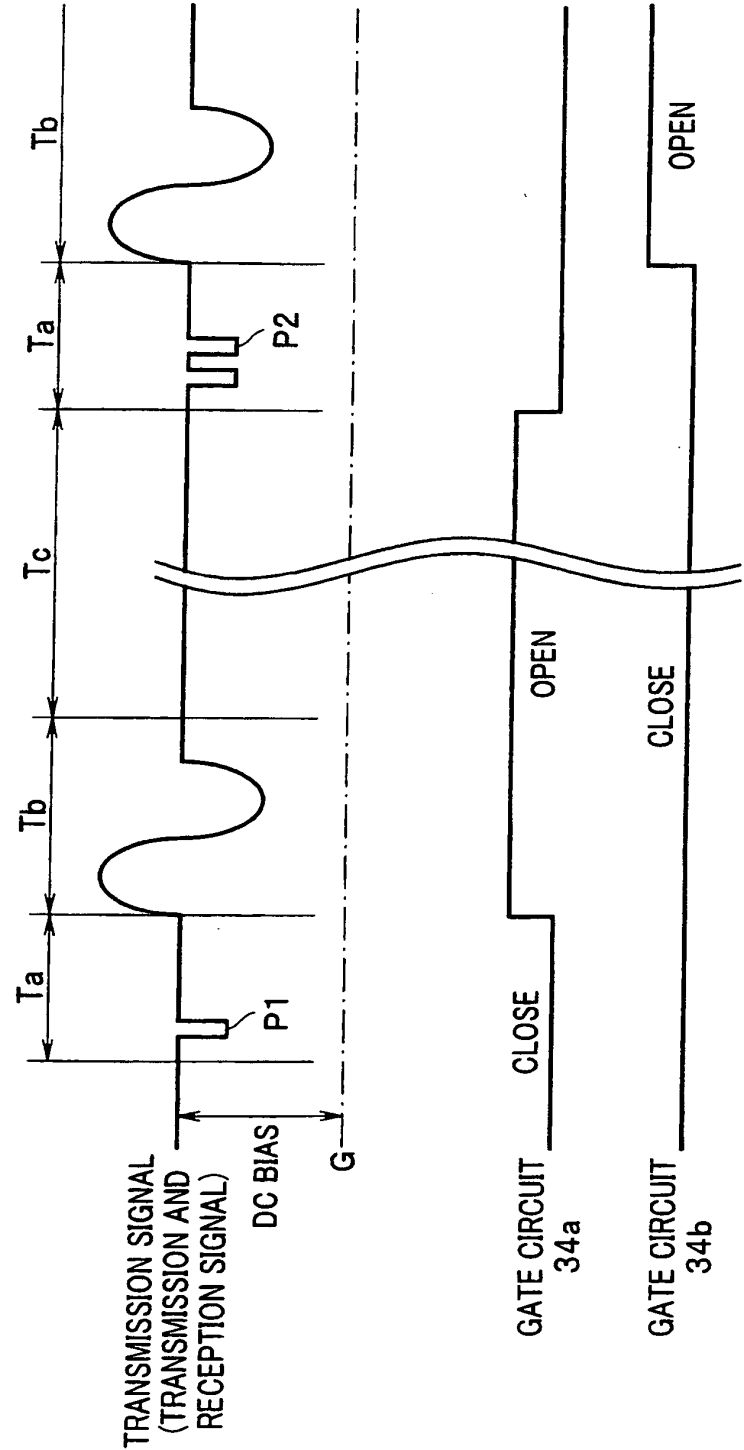


FIG.6

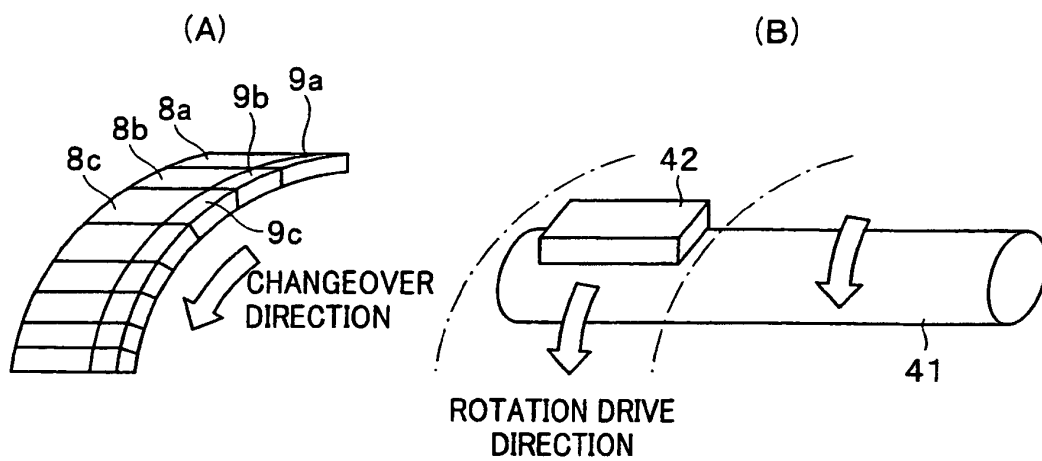


FIG. 7

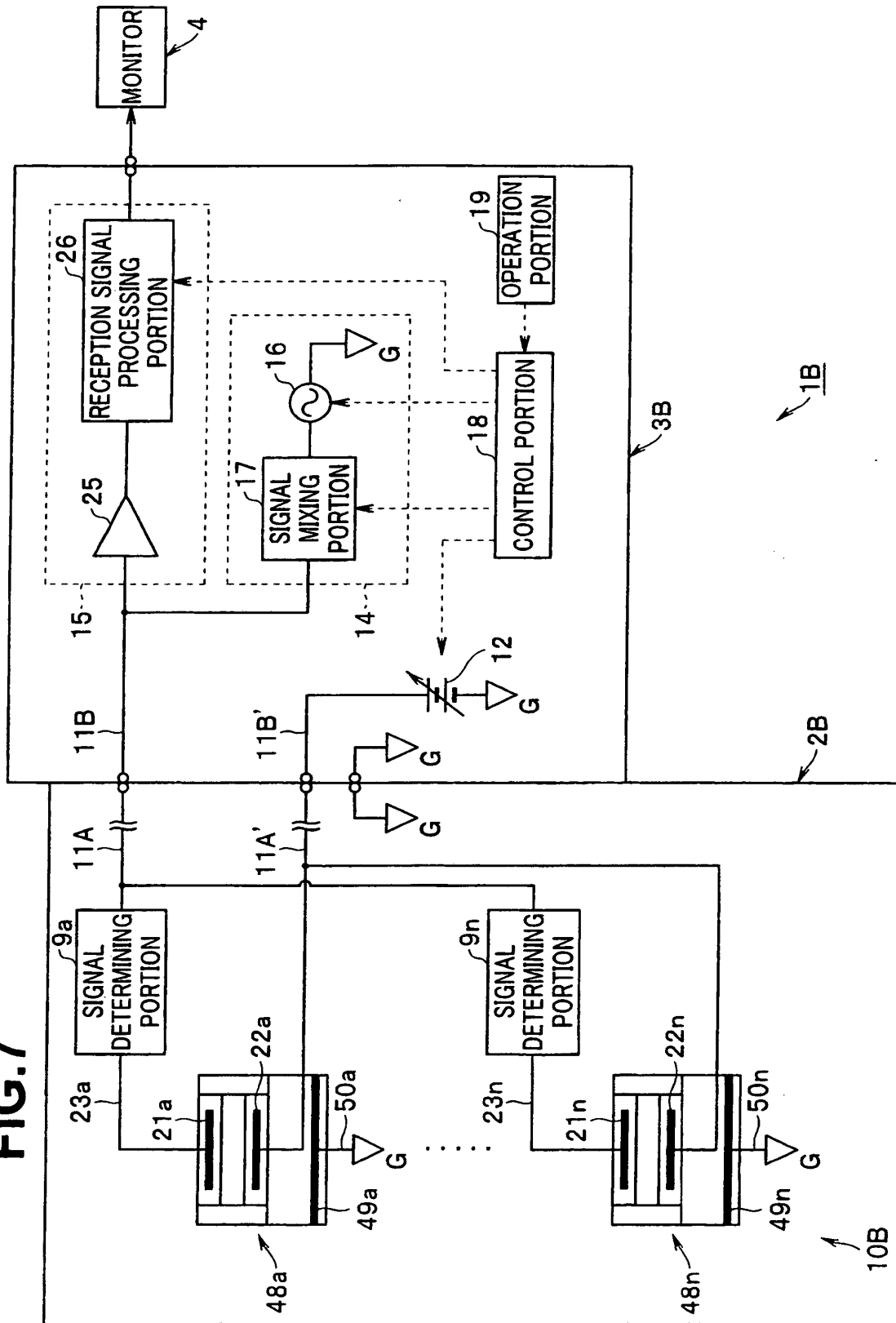


FIG.8

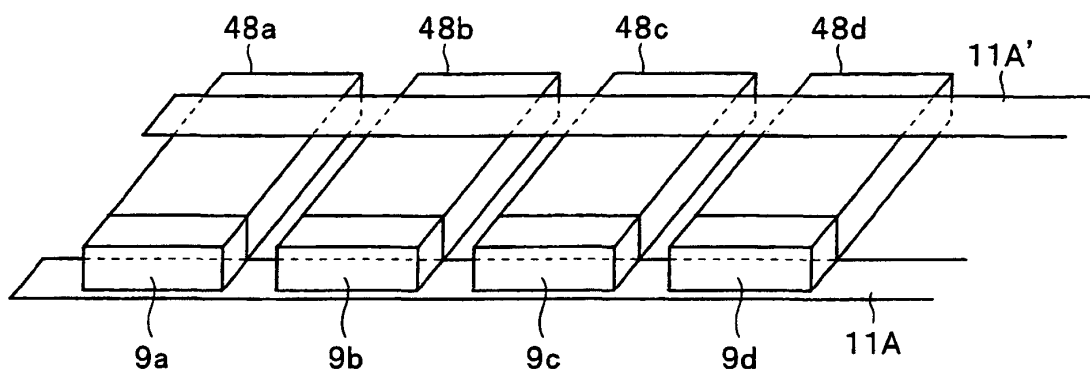


FIG.9

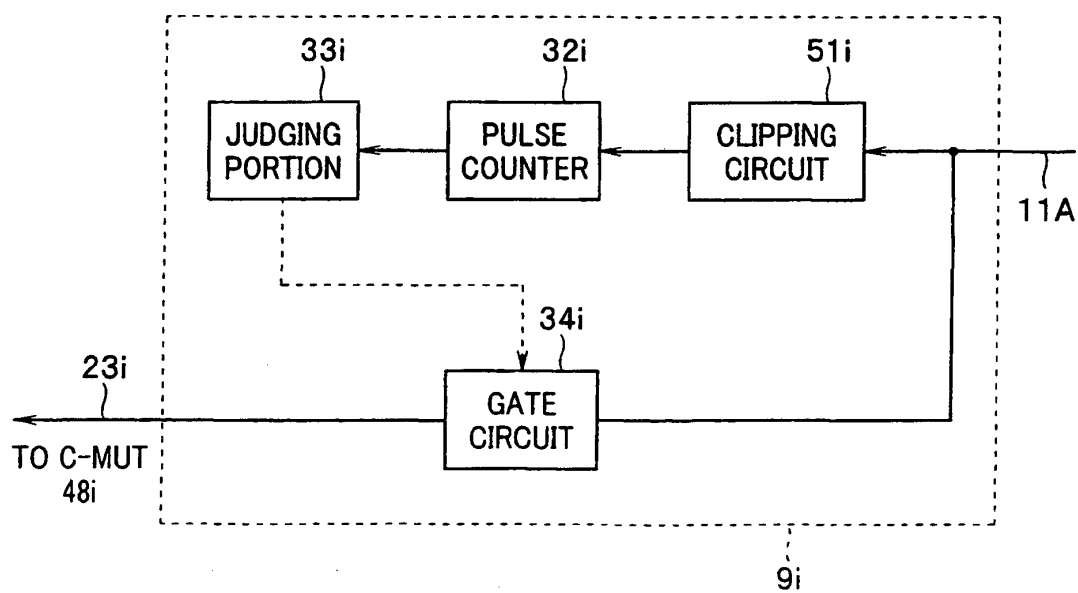


FIG.10

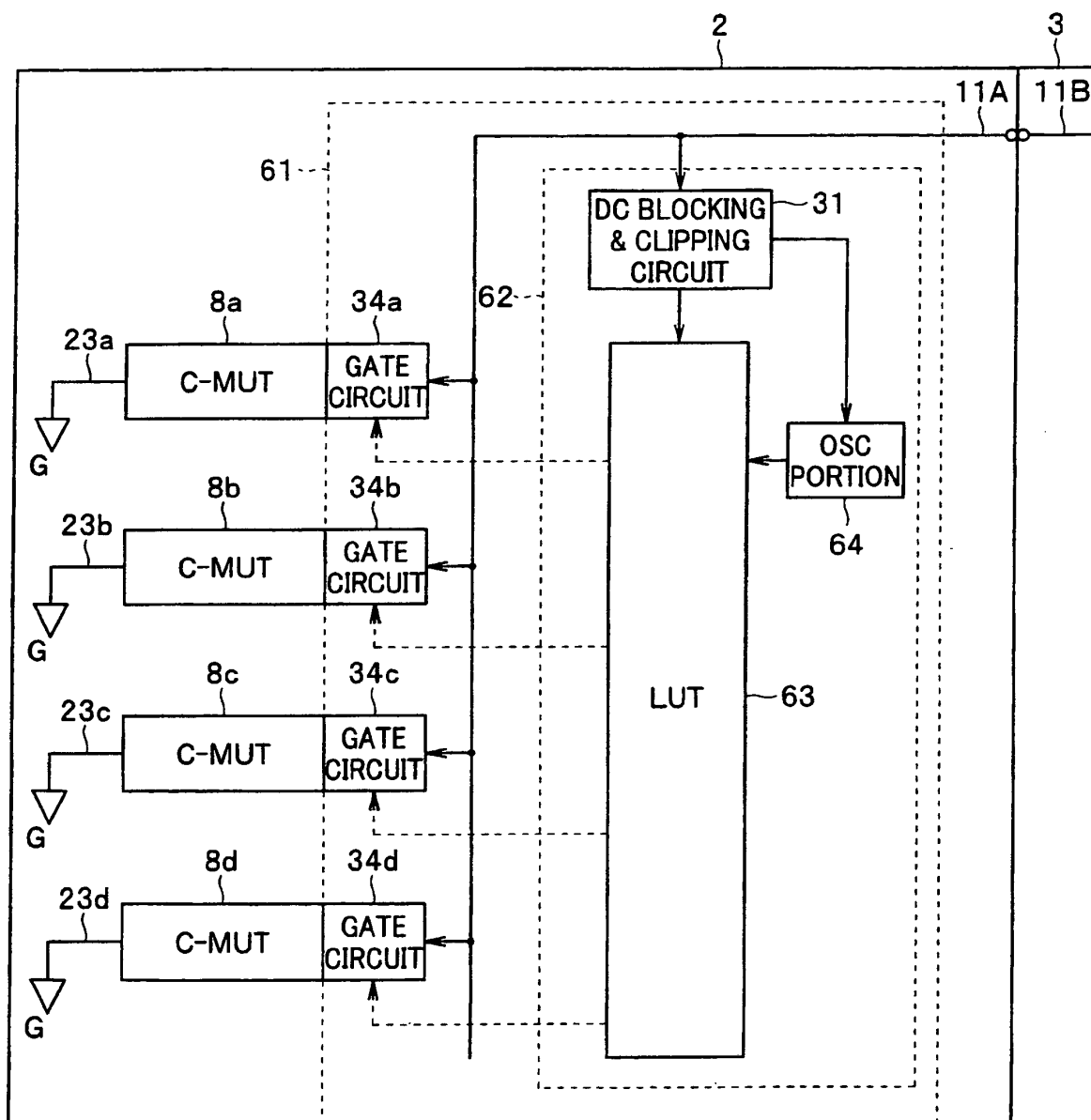


FIG.11

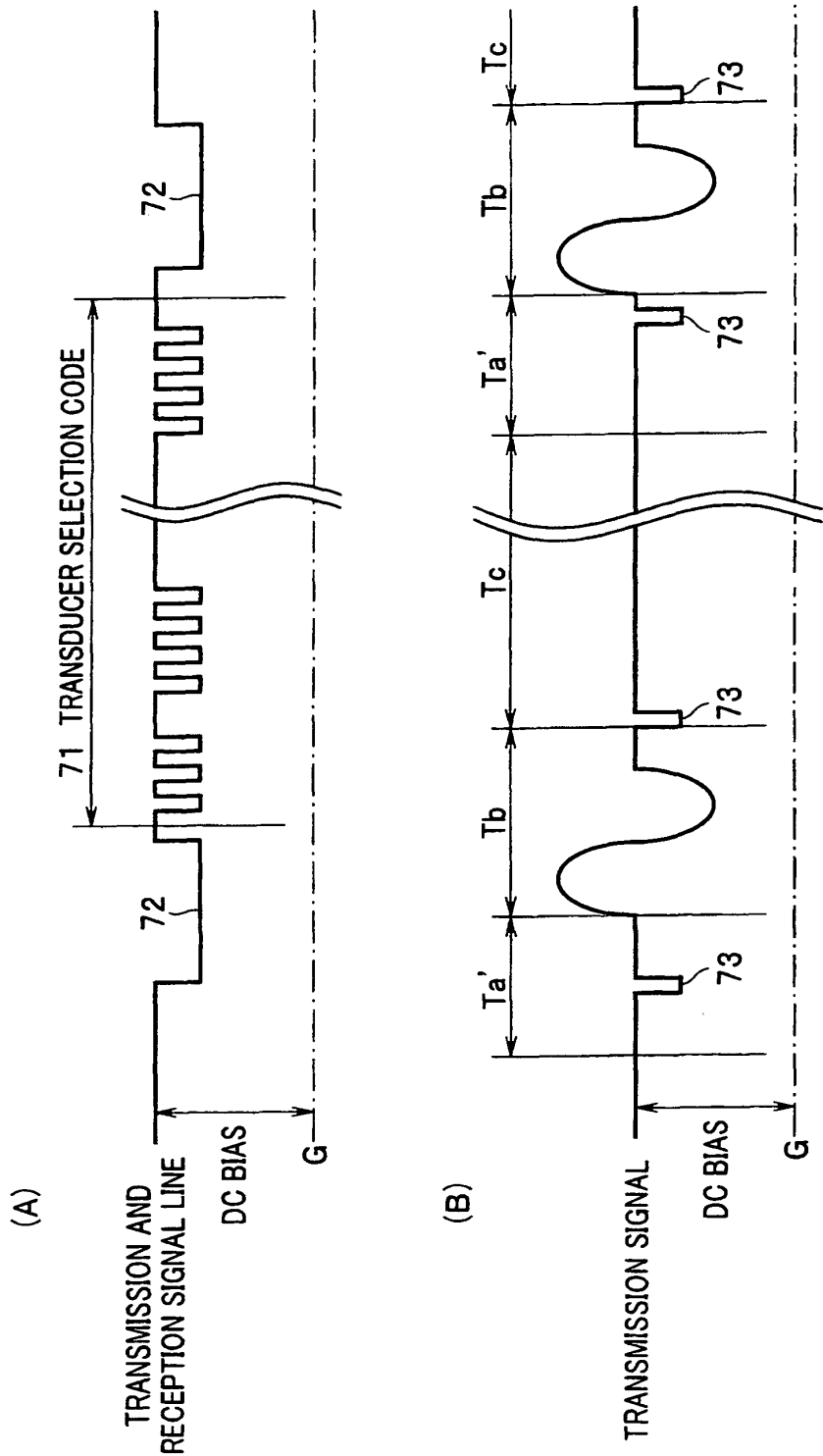


FIG.12**(A) SET PATTERN A**

CLK No	TRANSMISSION/ RECEPTION	SELECTED C-MUT
1	TRANSMISSION	8a
2	RECEPTION	8a
3	TRANSMISSION	8b
4	RECEPTION	8b
⋮	⋮	⋮

(B) SET PATTERN B

CLK No	TRANSMISSION/ RECEPTION	SELECTED C-MUT
1	TRANSMISSION	8a, 8b, 8c, 8d
2	RECEPTION	8a
3	TRANSMISSION	8a, 8b, 8c, 8d
4	RECEPTION	8b
⋮	⋮	⋮

FIG.13

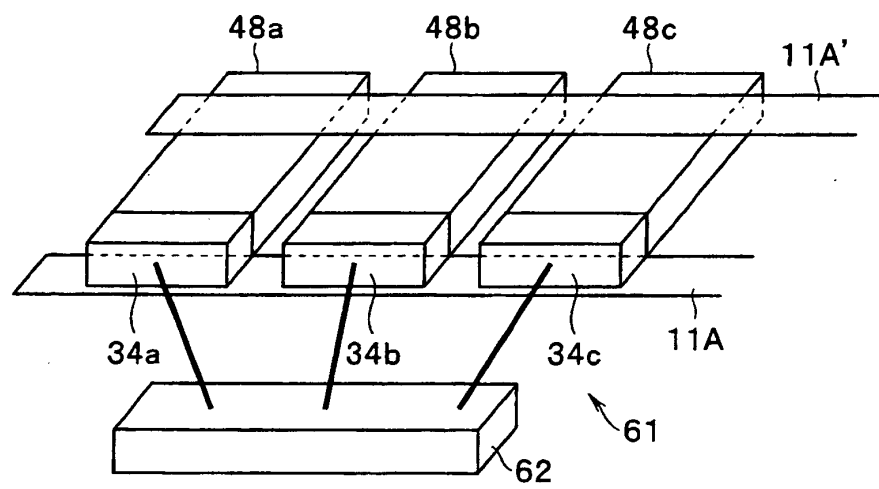


FIG.14

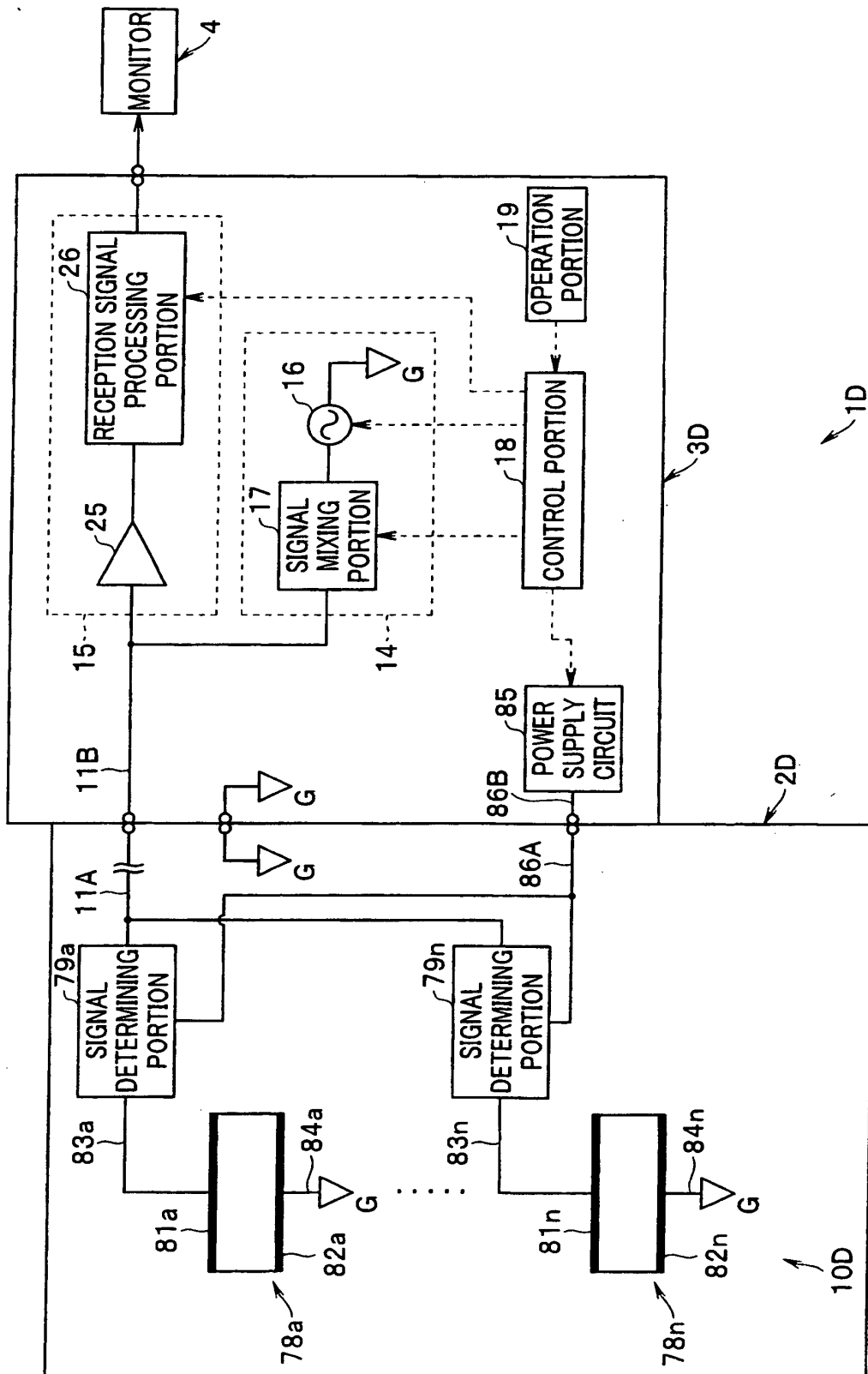
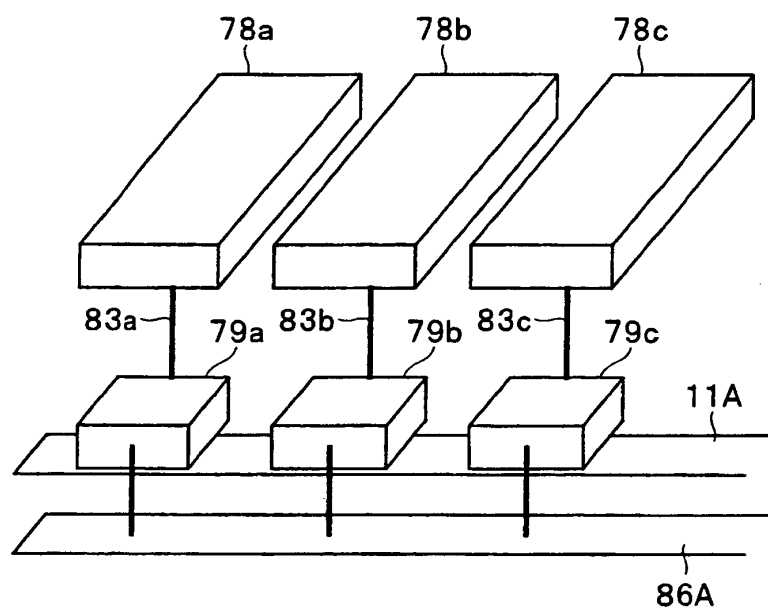


FIG.15



REFERENCES CITED IN THE DESCRIPTION

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- US 2001021072 A [0007]
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专利名称(译)	超声波诊断装置		
公开(公告)号	EP2454998B1	公开(公告)日	2014-12-31
申请号	EP2011814427	申请日	2011-07-14
[标]申请(专利权)人(译)	奥林巴斯医疗株式会社		
申请(专利权)人(译)	奥林巴斯医疗系统股份有限公司.		
当前申请(专利权)人(译)	奥林巴斯医疗系统股份有限公司.		
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IPC分类号	A61B8/12 A61B8/00		
CPC分类号	A61B8/12 A61B8/145 A61B8/445 A61B8/4461 A61B8/4477 A61B8/4483 A61B8/483 A61B8/56		
优先权	2010177876 2010-08-06 JP		
其他公开文献	EP2454998A4 EP2454998A1		
外部链接	Espacenet		

摘要(译)

一种超声波诊断装置，包括：发送和接收信号线，其将超声波的发送和接收信号发送到多个超声波换能器；信号确定部分靠近多个超声换能器并确定用于选择要驱动的超声换能器的选择信号或用于读出选择信号的读出信号，该选择信号与用于传输的信号同步地发送出去形成发送和接收信号，并根据确定结果将要驱动的超声换能器与发送和接收信号线电耦合。发送和接收信号线用选择信号或读出信号发送发送和接收信号。

FIG.1

