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(54) **Dual mode ultrasound system**

(57) A dual mode ultrasound system is described which comprises a mode selection switch (20) operable to select either a linear mode of scanning or a sector mode of scanning, an ultrasound transducer including a curved array of transducer elements having a front face, and a beamformer, responsive to the mode selection switch and coupled to the elements of the curved array, and operable in a first linear mode to cause the curved array to transmit and receive beams normal to the face of the array, and operable in a second sector mode to cause the curved array to transmit and receive beams emanating from a common apex.

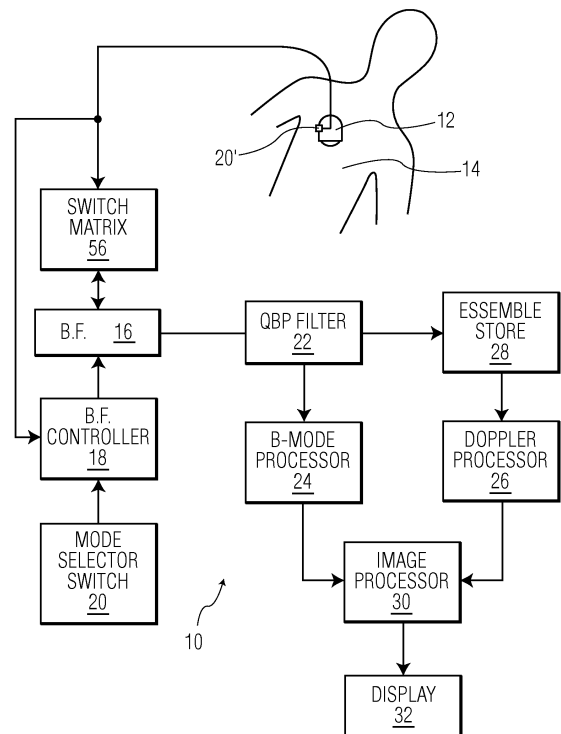


FIG. 3

Description

[0001] This invention relates to ultrasound systems, and, more particularly, to dual mode ultrasound systems.

[0002] In ultrasound diagnostic imaging, ultrasonic energy is emitted into a patient's body. The reflected energy is detected and processed to form images indicating the density and boundaries of tissue and the location and velocity of blood flow within the patient. Ultrasonic signals are typically emitted from a transducer including an array of individual piezoelectric transducer elements that also serve to detect the reflected signals.

[0003] Various transducers and scanning modes may be used to emit and receive the ultrasonic signals. In phased array imaging, multiple transducer elements emit signals having a phase and amplitude relationship such that they combine to form a single beam that can be steered to scan a pie-shaped sector viewing area. Sector mode imaging is particularly useful for imaging beneath a patient's ribs inasmuch as the beams can originate from a common vertex aimed between the patient's ribs, rather than a broader aperture emitting and receiving signals that can be blocked by the ribs.

[0004] In linear array scanning, a array of transducer elements sequentially emits signals from different groups of elements and receives signals from a viewing area within a patient. Linear arrays are typically used in applications requiring a wide view of a region close to the skin surface, and where acoustic access to the region of interest is not obstructed. Linear arrays are either flat or curved. A flat linear array provides a rectangular or trapezoidal field of view, while a curved linear provides a field of view that fans out due to the curvature of the array.

[0005] In practice, a technician will often need to have multiple transducers in order to adequately image different anatomies of a patient, which increases the cost of the ultrasound system. The technician will also need to switch the system operation from one transducer to another, which takes time. Inasmuch as transducers are used with a sound-conducting gel applied to the patient, each transducer therefore needs to be cleaned after use, requiring more time.

[0006] In view of the foregoing, it would be advantageous to provide an ultrasound transducer suitable for performing both sector and curved linear array scanning.

[0007] In accordance with the principles of the present invention, an ultrasound system includes a transducer having a face with a central portion and lateral portions on either side of the central portion. A first plurality of transducer elements are disposed on the central portion and a second plurality of transducer elements disposed on the lateral portions. The first plurality of transducer elements have a first, fine pitch for sector mode and the second plurality of transducer elements have a second, coarser pitch for linear mode. The array can be either curved or planar.

[0008] In sector mode, a beamformer is coupled to operate the transducer elements of the first plurality for

phased array imaging. In linear mode, the beamformer is coupled to operate the transducer elements of both groups. In accordance with a further aspect of the present invention, pairs of adjacent transducers of the first plurality may be operated in tandem so that the transducer will exhibit a common element pitch over the full operable aperture.

[0009] In another aspect of the invention, the number of transducer elements of the first plurality that are activated in sector mode is varied according to the number of transducer elements in contact with the patient's skin.

[0010] In another aspect of the invention, a mode selection switch is provided enabling a user to switch between linear and sector modes.

Figure 1 is a block diagram of an ultrasound system in accordance with an embodiment of the present invention.

Figures 2A and 2B are schematic diagram of a transducer face in accordance with an embodiment of the present invention.

Figure 3 is a schematic block diagram of an alternative embodiment of an ultrasound system in accordance with an embodiment of the present invention.

Figures 4A and 4B are schematic diagrams of control lines coupled to transducer elements in accordance with an embodiment of the present invention.

Figure 5A and 5B are schematic diagrams of a switch matrix coupling control lines to transducer elements in accordance with an embodiment of the present invention.

Figure 6 is a process flow diagram of a method for using a dual mode transducer in accordance with an embodiment of the present invention.

Figure 7 is a schematic diagram of a curved transducer engaging a patient's skin in accordance with an embodiment of the present invention.

Figure 8 is a schematic diagram of a switch matrix enabling a variable transducer aperture in accordance with an embodiment of the present invention.

Figure 9 is a process flow diagram of a method for using a transducer having a variable aperture in accordance with an embodiment of the present invention.

[0011] Referring to Figure 1, an ultrasound system 10 includes a transducer 12 having a number of transducer elements suitable for transmitting ultrasonic signals into a patient and receiving echo signals. The transducer elements are preferably piezoelectric transducer elements. The transducer 12 is coupled to a beamformer 16 which is controlled by a beamformer controller 18. The beamformer 16 controls the phase and amplitude of excitation signals applied to the elements of the transducer 12 to create ultrasound beams scanning a viewing area within a patient. The beamformer 16 also relatively delays the phase of signals received by the transducer elements to bring the signals into phase coherence and

then sums them. In the illustrated embodiment, a mode selector switch 20 is coupled to the beamformer controller 18 so that the user can set the beamformer operation for scanning with the transducer 12 in a sector mode, linear mode, and other operational modes. In other embodiments the mode selector switch 20' is located on the case of the transducer. In yet other embodiments, the mode selector switch is provided by a graphical user interface coupled to the beamformer controller 18.

[0012] The output of the beamformer 16 is filtered to extract information from the echo signal. In the illustrated embodiment, a quadrature bandpass filter 22 is used. The output of the filter 22 is provided to one or both of a B-mode processor 24 and a Doppler processor 26. The B-mode processor 24 processes the data to produce information regarding the structure of the tissue that reflected the excitation signal. The Doppler processor 26 processes the data to extract information regarding the velocity of blood flow within the viewing area. Data provided to the Doppler processor 26 may be stored in an ensemble store 28 before being processed by the Doppler processor 26 until sufficient samples of the viewing area have been acquired to form a Doppler image. The outputs of the B-mode processor 24 and Doppler processor 26 are provided to an image processor 30 that creates B-mode and Doppler images of the desired image format, which are then displayed on a display 32.

[0013] Referring to Figures 2A and 2B, the transducer 12 has a face 34 that is convex, having a center of curvature 36 located behind the face 34 and having a plurality of transducer elements 38 distributed along the face 34. The transducer elements 38 located on a central portion 40 of the face 34 have a first pitch 42 and the transducer elements 38 located on lateral portions 44 on either side of the central portion 40 have a second pitch 46 that is greater than the first pitch. In a preferred embodiment, the second pitch 46 is twice the first pitch 42. The combined number of transducer elements 38 on the lateral portions 44 may be equal to one half the number of transducer elements 38 on the central portion 40. The different pitches in the central portion 40 and the lateral portions 44 may be obtained by dicing a piezoelectric crystal at different lateral increments along the face 38.

[0014] The transducer elements emit an ultrasound wave with a wavelength λ . The first pitch 42 may be less than or about equal to $\lambda/2$ whereas the second pitch 46 is less than or about equal to λ . The different pitches 42, 46 facilitate use of the transducer 12 to perform different types of ultrasound scans.

[0015] Referring specifically to Figure 2A, in a linear scanning mode, the transducer elements 38 are activated sequentially to emit ultrasound beams 48 normal to the face 34. In the linear mode, the transducer elements 38 in the central portion 40 are preferably excited in pairs 50 such that the angular distribution of ultrasound beams 48 is constant.

[0016] Referring specifically to Figure 2B, in a phased array beam-steering mode, the excitation signals applied

to the finer pitched elements 38 have phases and amplitudes chosen such that the ultrasound signals emitted from the elements 38 combine to form a focused beam 52 during each transmission. The phases and amplitudes are varied to change the angle of each beam 52 and perform a sector scan of the viewing area. In the illustrated embodiment, the beams 52 extend from an apex 54 located at the face 34 of the transducer. However, the apex 54 may be located at other positions by changing the steering angle, such as in front or behind the face 34. In a preferred embodiment, only the transducer elements 38 of the central portion 40 are used to generate the beams 52 in the beam-steering mode. The finer pitch 42 in the central portion 40 advantageously allows for a greater range of steering angles as compared to a larger pitch without creating grating or significant side lobes or other artifacts that degrade image quality.

[0017] Referring to the embodiment of Figure 3, a switch matrix 56 is interposed between the beamformer 16 and the elements of transducer 12. The switch matrix 56 changes the coupling between signal lines of the beamformer 16 and the transducer elements 38 of the transducer 12 according to a mode selected by the operator. In an alternative embodiment, the signals applied to the transducer elements 38 are controlled programmatically to switch between modes, such as by the beamformer controller 18, without changing the coupling between the beamformer 16 and the transducer elements 38.

[0018] For example, referring to Figures 4A, the switch matrix 56 may couple control lines 58 from the beamformer 16 to individual transducer elements 38 of the central portion 40 in the sector mode. Referring to Figure 4B, in the linear mode, the switch matrix 56 couples the control lines 58 to the transducer elements 38 of the lateral portions 44 and to pairs 50 of transducer elements 38 in the central portion 40. In the embodiment of Figures 4A and 4B, the number of control lines 58 is less than the total number of transducer elements 38. In the illustrated embodiment, the number of control lines 58 is equal to the number of transducer elements 38 in the central portion, which is two thirds of the total number of transducer elements 38. In other embodiments, the number of control lines is equal to the total number of transducer elements 38. In some embodiments, 128 control lines 58 are used. Accordingly, the transducer 12 may include 128 transducer elements 38 in the central portion 40 and 32 transducer elements per lateral portion 44 for a total of 64 located in the lateral portions.

[0019] Referring to Figures 5A and 5B, in this embodiment the control lines 58 are coupled to the transducer elements 38 as illustrated. The illustrated coupling between the control lines 58 and the transducer elements 38 may be described mathematically by assigning each control line 58 a number (n) and assigning each transducer element 38 a number (i) corresponding to their position relative to the center 60 of the transducer 12. In sector mode, each control line n is coupled to transducer

$i=n$ of the central portion 40, as shown in Figure 5A. In linear mode, each control line n is coupled to two transducer elements $i=2n-1$ and $i=2n$ in the central portion 40 and transducer element $i=N/2+n$ in the lateral portions 44, where N is equal to one half of the number of transducer elements 38 in the central portion 40, as shown in Figure 5B.

[0020] Stated differently, each transducer element i in the central portion is coupled to control line $n=i$ in sector mode and control line $n=i - \text{INT}(i/2)$ in linear mode, where the $\text{INT}()$ function returns the integer portion of its operand. Where i is equal to one, $i - \text{INT}(i/2)$ is equal to one. Accordingly, transducer elements $i=1$ are coupled to control line $n=1$ in both sector and linear modes and no switching is needed. The remaining transducer elements $i+1$ 1 to N of the central portion 40 are each coupled to the control lines 58 by two switches 62a, 62b, only one of which is closed at a time. Switch 62a is closed in the sector mode and couples transducer element i to control line $n=i$ as shown in Figure 5A. Switch 62b is closed in linear mode and couples transducer element i to control line $n=i-\text{INT}(i/2)$, as shown in Figure 5B. Switches 64 couple the transducer elements 38 of the lateral portions 44 to the control lines $n=N+1$ to $n=N+M$ in linear mode, where M is the number of transducer elements 38 in an individual lateral portion 44. The switches 64 are closed in the linear mode and open in the sector mode.

[0021] Referring to Figure 6, a method 66 for performing ultrasound scans may include coupling control lines to the transducer elements 38 of a central portion 40 of a transducer 12 at step 68. At step 70, one or more sector scans of a viewing area within a patient 14 are performed using the ultrasound system 10. At step 72, a user mode selection input is received from the user by means of a mode selection switch 20, graphical user interface, or other input means.

[0022] Where the mode selection input indicates selection of a linear scanning mode, the method 66 includes coupling pairs of transducer elements 38 of the central portion 40 to a portion of the control lines at step 74. At step 76, another portion of the control lines are coupled to the transducer elements 38 of the lateral portions 44. At step 78, a linear scan is performed. The steps of the method 66 may be reordered such that a user mode selection input indicating a sector mode causes the ultrasound system 10 to execute steps 68 and 70.

[0023] In order to properly image a viewing area within a patient 14, it is typically necessary to reduce air gaps between the transducer 12 and the patient's skin. This is typically accomplished by placing a sound-conducting gel on the patient's skin in order to fill gaps and provide a good sound-conducting layer between the transducer 12 and the patient's skin. When the front face 34 is convex, not all of the transducer elements 38 may adequately contact the patient's skin or the sound-conducting gel in some uses. For example, when imaging through a patient's ribs, the ribs may not allow the transducer 12 to be pressed into the patient 14 sufficient to make good

contact with all of the transducer elements of the central portion 40. Accordingly, in some embodiments, the number of transducer elements 38 within the central portion 40 that are activated in sector mode may be reduced according to the number of transducer elements 38 in contact with the patient's skin or the sound-conducting gel.

[0024] Thus, as shown in Figure 7, where a first area 80 of the central portion 40 makes adequate contact with the patient's skin 82 then the transducer elements 38 within the area 80 will be activated to produce the steered beam. Where a smaller area 84 contacts the patient's skin 82', only the transducer elements 38 of the smaller area 84 are activated.

[0025] Referring to Figure 8, reducing the number of transducer elements 38 used in sector mode may include opening some of the outermost switches 62a in sector mode, as illustrated, such that the outer transducers 38 of the central portion 40 are not coupled to the beamformer 16.

[0026] Referring to Figure 9, a method 86 for accommodating different patient skin compliance may include performing an initial scan at step 88. In some embodiments, the initial scan includes sequentially emitting from each transducer element 38 such that an echo signal can be readily associated with each transducer element. At step 90, the output of the transducer elements 38 are analyzed to determine which of the transducer elements are not adequately engaged with the patient 14 or sound-conducting gel. Determining which of the transducer elements is not adequately engaged may include analyzing the echo signal received for each transducer element 38 and comparing the intensity of the reflected signal to a threshold to determine if adequate sound reception is occurring. At step 92, transducer elements 38 for which no signal or a below-threshold echo signal are received are identified as not adequately engaging the patient 14 or the sound-conducting gel. The identifying step 92 may be performed automatically or by an operator presented with an ultrasound image representing the echo signals from the initial scan. At step 94, the transducer elements 38 identified as not adequately engaging the patient or the sound-conducting gel are decoupled from the beamformer 16, reducing the active aperture for this scan. The decoupling step of step 94 may be performed automatically or by an operator. For example, an operator may turn a dial or interact with a graphical user interface element to indicate to the beamformer controller 18 which transducer elements 38 are to be decoupled or used in the active aperture. As an alternative to step 94, the beamformer 16 may be programmed to refrain from using signals in beamforming from elements identified as being inadequately acoustically coupled to the patient, rather than decoupling them from control lines. At step 96, one or more beam steered scans of the patient 14 is performed using the transducer elements 38 that are adequately acoustically coupled to the patient 14.

[0027] Although the present invention has been de-

scribed with reference to the disclosed examples, persons skilled in the art will recognize that changes may be made in form and detail without departing from the spirit and scope of the invention. Such modifications are well within the skill of those ordinarily skilled in the art. Accordingly, the invention is not limited except as by the appended claims.

Claims

1. An ultrasound system, comprising:

- a mode selection switch (20) operable to select either a linear mode of scanning or a sector mode of scanning;
- an ultrasound transducer (12) including a curved array of transducer elements having a front face; and
- a beamformer (16), responsive to the mode selection switch and coupled to the elements of the curved array, and operable in the linear mode to cause the curved array to transmit and receive beams normal to the face of the array, and operable in the sector mode to cause the curved array to transmit and receive beams emanating from a common apex.

2. The ultrasound system of claim 1 wherein in the linear mode the curved array is operated as a linear array and in the sector mode the curved array is operated as a phased array.

3. The ultrasound system of claim 2 wherein, in the linear mode, an active aperture for each beam is shifted along the face of the array from beam to beam, and in the sector mode, the same active aperture of transducer elements is used for phased array beam steering of each beam.

4. The ultrasound system of claim 1 wherein, in the sector mode, the signals from elements which are not acoustically coupled to a patient do not participate in beam formation.

5. The ultrasound system of claim 4, wherein elements which are not acoustically coupled to a patient are identified by comparing echo signals received by transducer elements to a threshold.

6. The ultrasound system of claim 4 further comprising an aperture control for adjusting the elements which contribute to the active aperture of the transducer.

7. The ultrasound system of claim 1 wherein, in the sector mode, the active aperture of the transducer comprises only transducer elements located in a central portion of the transducer array; and

- in the linear mode, the active aperture of the transducer comprises transducer elements located in the central portion of the transducer array and transducer elements located on both sides of the central portion.

8. The ultrasound system of claim 7, wherein the transducer elements of the central portion exhibit a finer pitch than that of the transducer elements on both sides of the central portion.

9. The ultrasound system of claim 8 wherein, in the linear mode, the transducer elements of the central portion are operated in pairs.

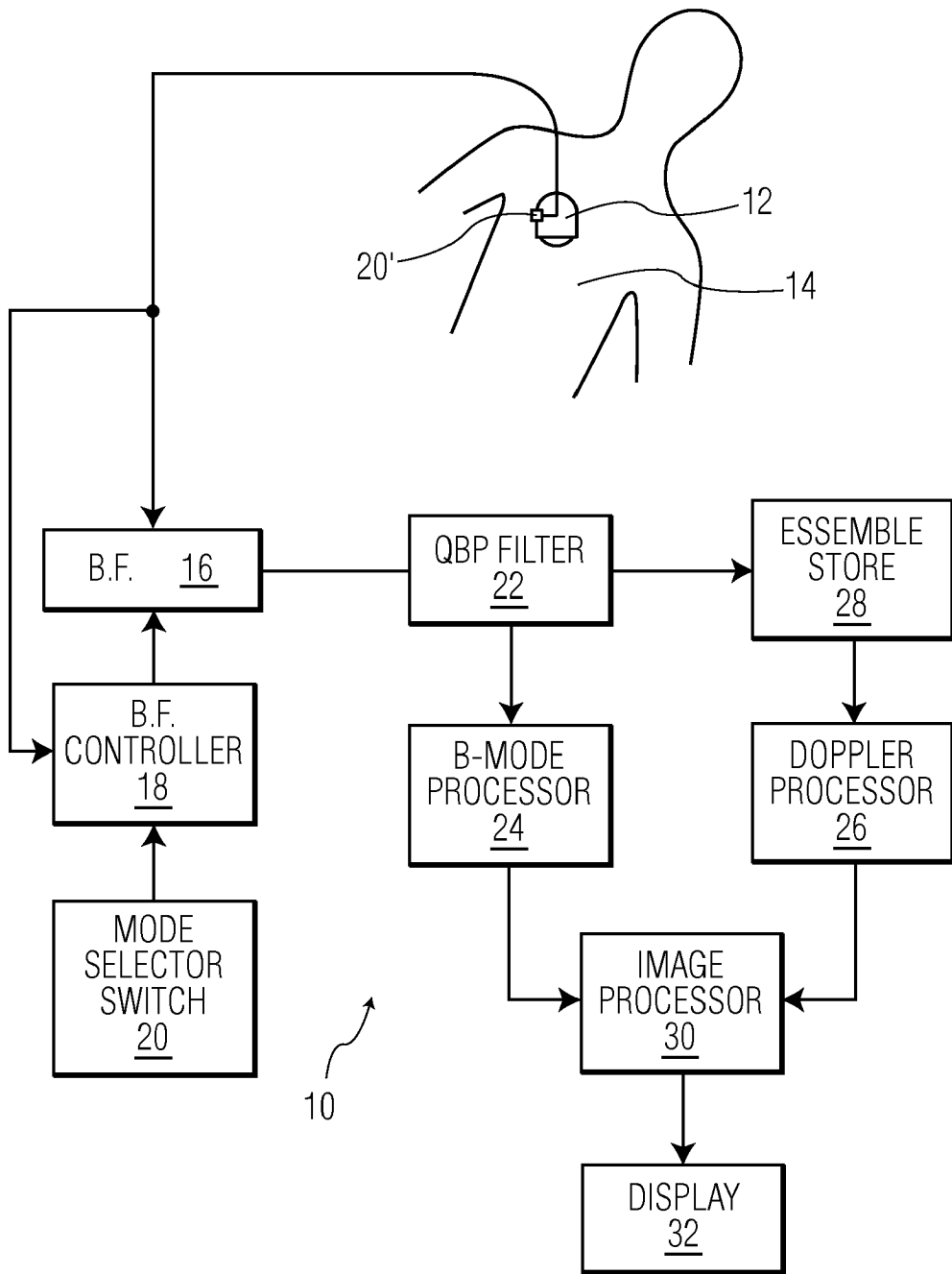


FIG. 1

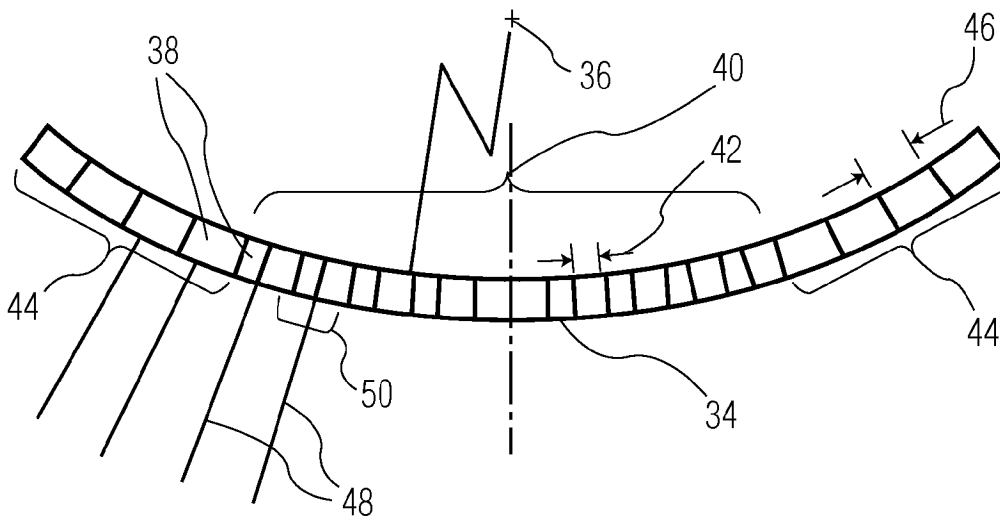


FIG. 2A

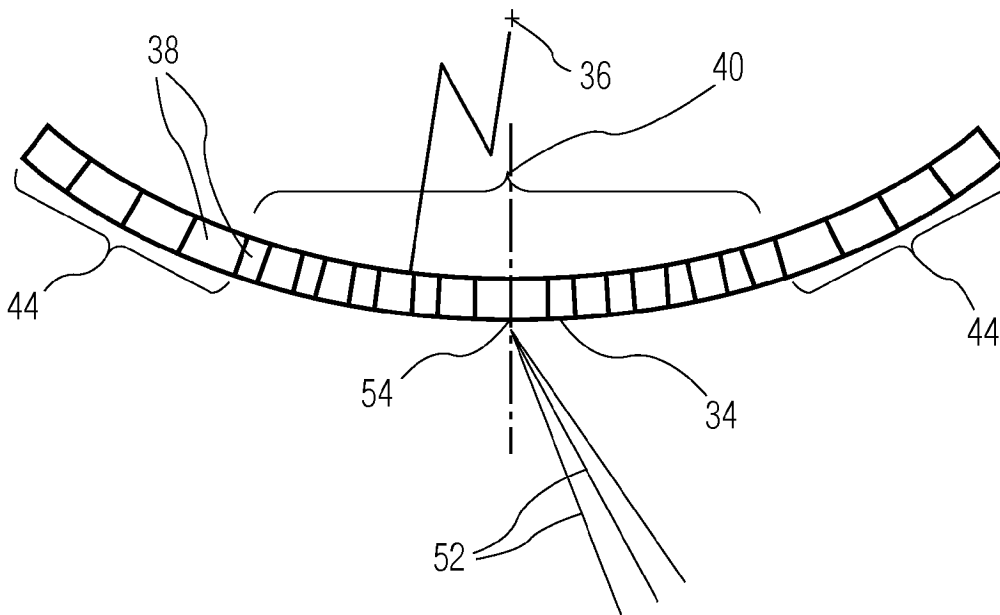


FIG. 2B

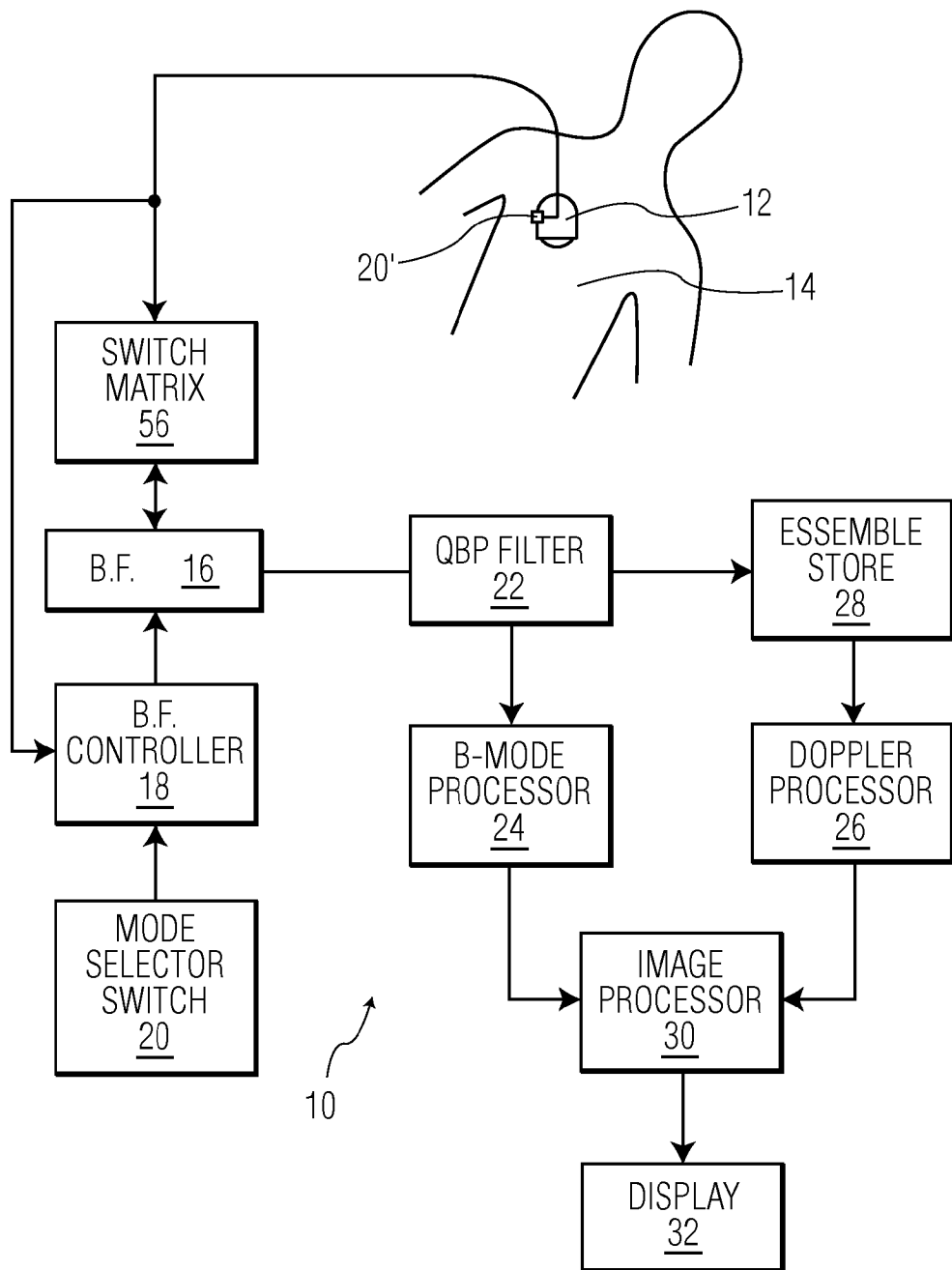


FIG. 3

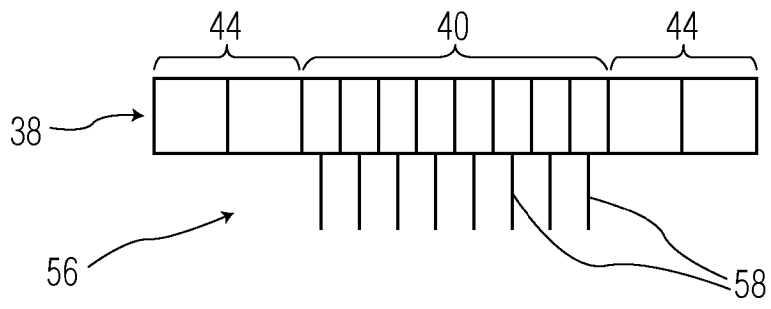


FIG. 4A

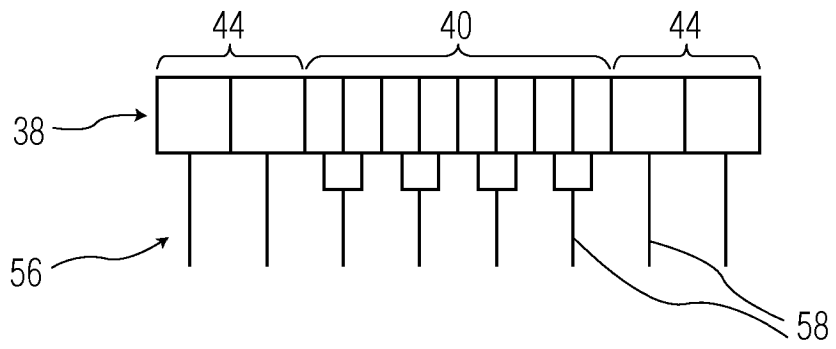


FIG. 4B

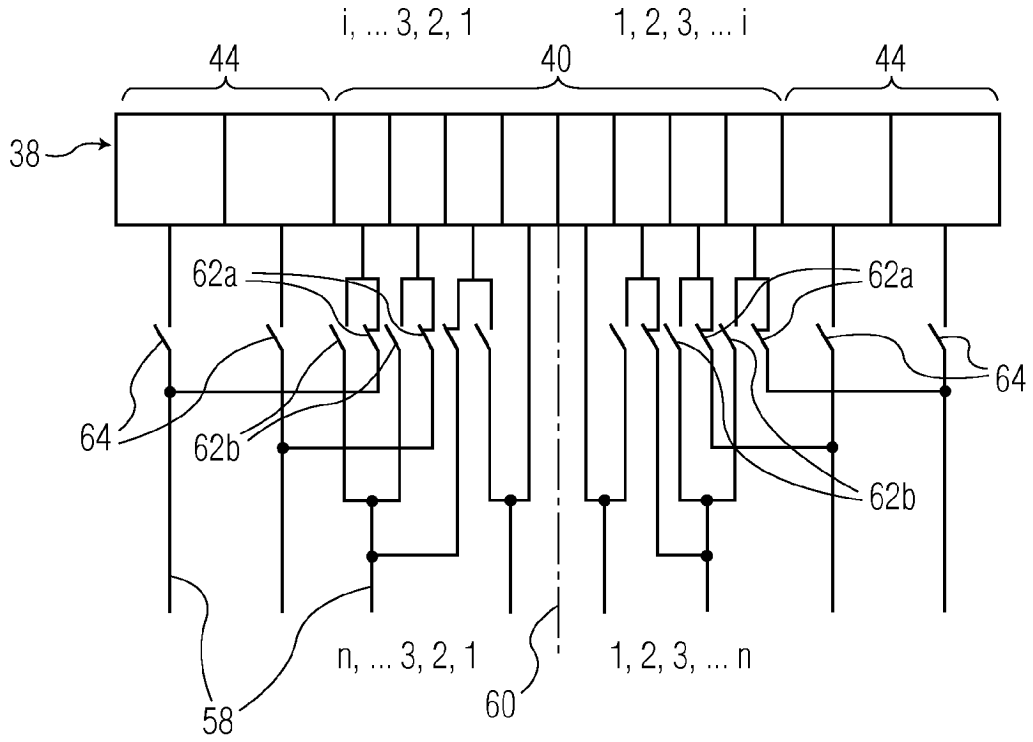


FIG. 5A

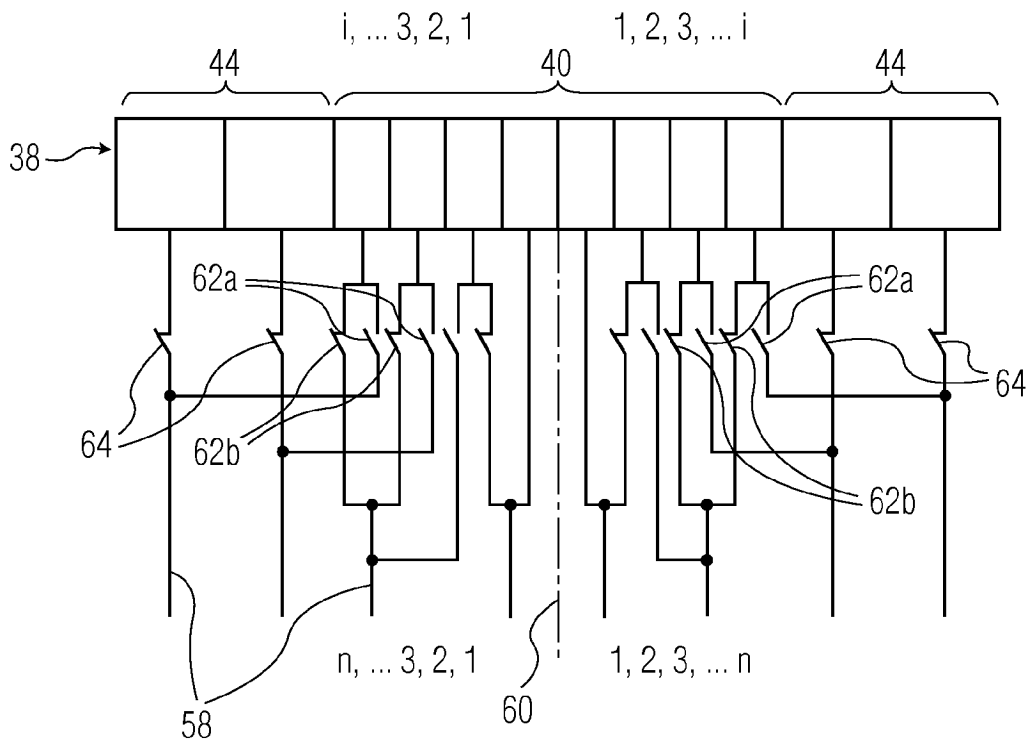


FIG. 5B

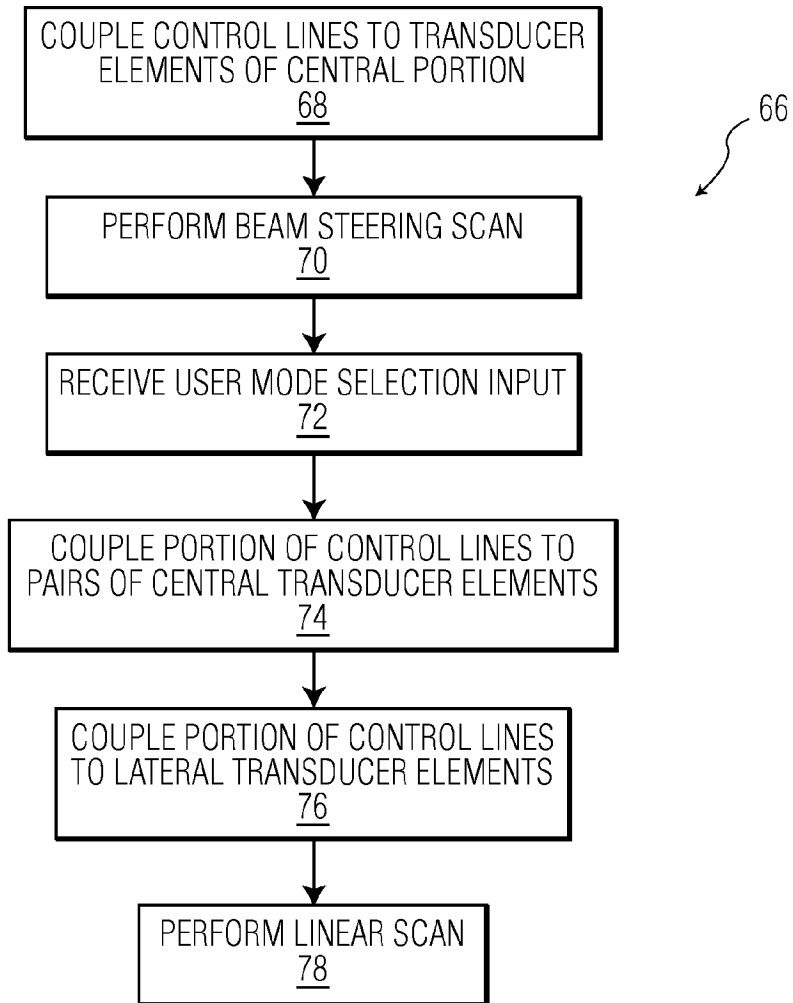


FIG. 6

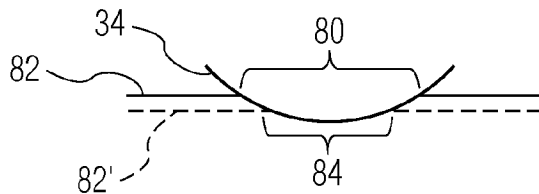


FIG. 7

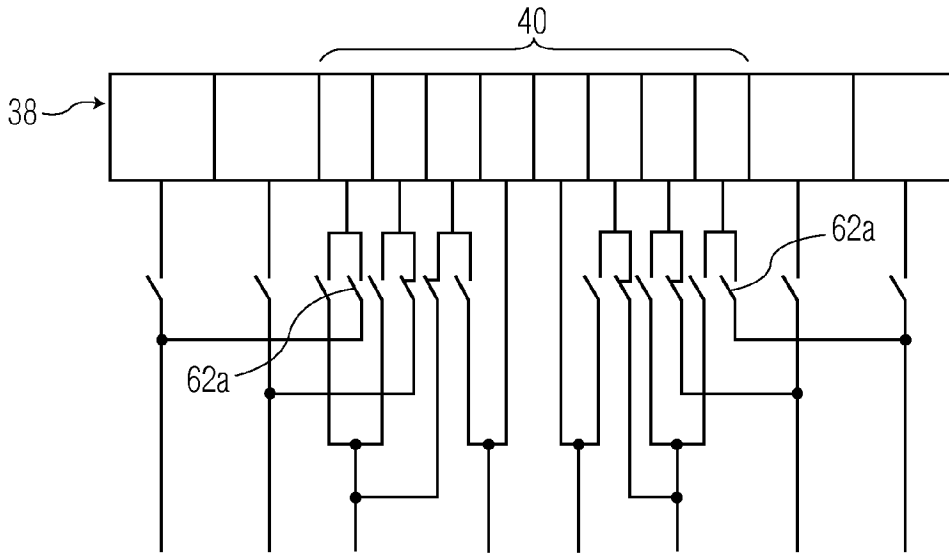


FIG. 8

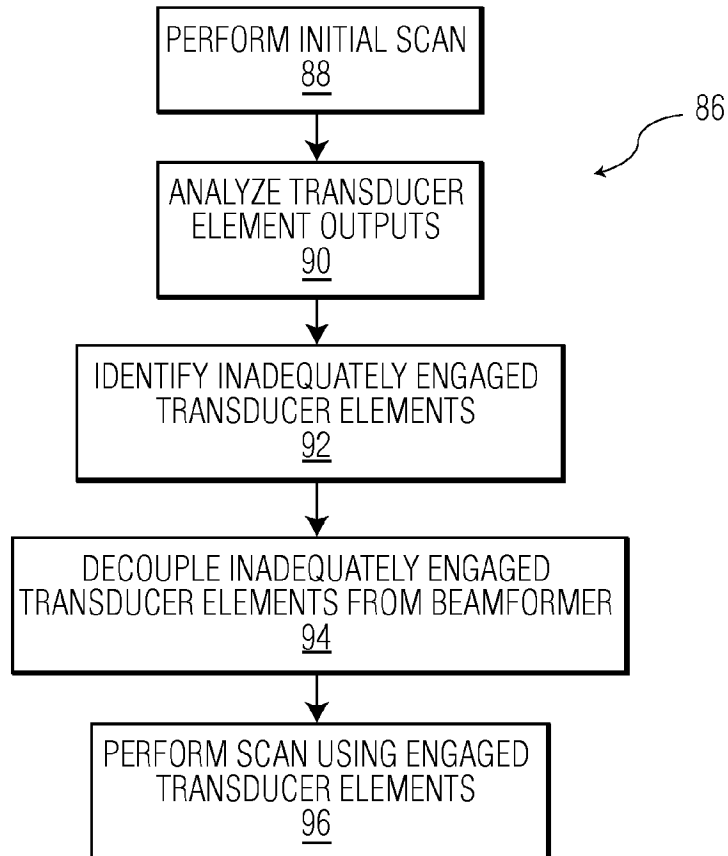


FIG. 9



EUROPEAN SEARCH REPORT

Application Number
EP 10 16 7347

DOCUMENTS CONSIDERED TO BE RELEVANT			
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (IPC)
X	US 6 106 472 A (CHIANG ALICE M [US] ET AL) 22 August 2000 (2000-08-22)	1-6	INV. G01S15/89 G10K11/34
Y	* abstract * * column 30, line 53 - column 31, line 3 * * column 31, line 29 - column 32, line 7 * * sentences 34-44, paragraph 32 * * figure 30b *	7-9	
X	----- US 6 104 673 A (COLE CHRISTOPHER R [US] ET AL) 15 August 2000 (2000-08-15)	1-6	
Y	* abstract * * column 9, lines 37-41 * * column 10, line 44 - column 11, line 38 * * figures 1,2 *	7-9	
A	----- US 2006/058672 A1 (KLEPPER JOHN R [US]) 16 March 2006 (2006-03-16)	1-9	
A	* paragraphs [0018], [0026], [0033] *	1-9	
A	----- US 4 550 607 A (MASLAK SAMUEL H [US] ET AL) 5 November 1985 (1985-11-05)	1-9	TECHNICAL FIELDS SEARCHED (IPC)
A	* abstract *	1-9	G01S G10K
A	----- US 5 798 461 A (BANTA JR ROBERT H [US] ET AL) 25 August 1998 (1998-08-25)	1-9	
A	* abstract * * figure 6 *	1-9	
A	----- US 4 664 122 A (YANO MASAHIKO [JP]) 12 May 1987 (1987-05-12)	1-9	
	* abstract * * figure 2 *		

1 The present search report has been drawn up for all claims			
Place of search		Date of completion of the search	Examiner
Munich		30 July 2010	Willig, Hendrik
CATEGORY OF CITED DOCUMENTS		T : theory or principle underlying the invention E : earlier patent document, but published on, or after the filing date D : document cited in the application L : document cited for other reasons	
X : particularly relevant if taken alone Y : particularly relevant if combined with another document of the same category A : technological background O : non-written disclosure P : intermediate document		& : member of the same patent family, corresponding document	

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ANNEX TO THE EUROPEAN SEARCH REPORT
ON EUROPEAN PATENT APPLICATION NO.

EP 10 16 7347

This annex lists the patent family members relating to the patent documents cited in the above-mentioned European search report. The members are as contained in the European Patent Office EDP file on
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30-07-2010

Patent document cited in search report		Publication date	Patent family member(s)	Publication date
US 6106472	A	22-08-2000	NONE	

US 6104673	A	15-08-2000	NONE	

US 2006058672	A1	16-03-2006	NONE	

US 4550607	A	05-11-1985	AT 78105 T	15-07-1992
			AU 575160 B2	21-07-1988
			AU 4202585 A	14-11-1985
			CA 1236210 A1	03-05-1988
			DE 3586294 D1	13-08-1992
			DE 3586294 T2	28-01-1993
			EP 0161587 A1	21-11-1985
			JP 1651941 C	30-03-1992
			JP 3018456 B	12-03-1991
			JP 61022847 A	31-01-1986

US 5798461	A	25-08-1998	NONE	

US 4664122	A	12-05-1987	JP 61031135 A	13-02-1986

EPO FORM P0459

For more details about this annex : see Official Journal of the European Patent Office, No. 12/82

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[标]申请(专利权)人(译)	皇家飞利浦电子股份有限公司		
申请(专利权)人(译)	皇家飞利浦电子N.V.		
当前申请(专利权)人(译)	皇家飞利浦电子N.V.		
[标]发明人	ADAMS DARWIN		
发明人	ADAMS, DARWIN		
IPC分类号	G01S15/89 G10K11/34 A61B8/00 B06B1/06		
CPC分类号	A61B8/00 G01S15/8918 G01S15/892 G01S15/8927 G10K11/346		
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其他公开文献	EP2237070B1		
外部链接	Espacenet		

摘要(译)

描述了一种双模式超声系统，其包括模式选择开关（20），其可操作以选择线性扫描模式或扇形扫描模式，超声换能器包括具有正面的换能器元件的弯曲阵列，以及波束形成器响应于模式选择开关并耦合到弯曲阵列的元件，并且可在第一线性模式下操作以使得弯曲阵列发射和接收垂直于阵列面的光束，并且可在第二扇区模式下操作使弯曲的阵列发射和接收从共同的顶点发出的光束。

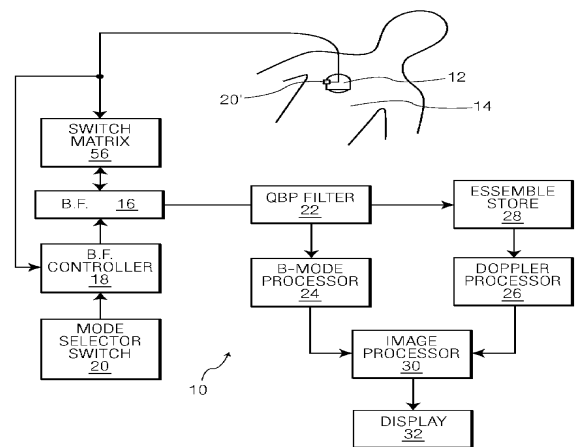


FIG. 3