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(54) **Apparatus for medical ultrasound navigation user interface**

Vorrichtung für eine Benutzerschnittstelle zur medizinischen Ultraschallnavigation

Dispositif pour une interface utilisateur pour navigation médicale ultrasonore

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(56) References cited:
WO-A-00/58754 WO-A-2004/029655
US-A- 5 315 999 US-A- 5 964 707
US-B1- 6 186 948

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Description

[0001] The present invention relates to diagnostic ultrasound systems. In particular, the present invention relates to systems for navigation in ultrasound data.

[0002] Numerous ultrasound methods and systems exist for use in medical diagnostics. Various features have been proposed to facilitate patient examination and diagnosis based on ultrasound images of the patient. For example, certain systems offer ultrasound volumetric imaging of an object, e.g. the human heart. To be useful, these systems require a navigator for orienting view planes within the volume data. Typically, the navigation of the view planes must be done after data acquisition.

[0003] Document WO-A-2004/029655 discloses an ultrasound system, which allows rotation of a displayed volume as the ultrasound data is being acquired in real time.

[0004] Heretofore, ultrasound methods and systems were unable to acquire volumetric ultrasound data at the same time as an operator navigates in the volumetric data to generate 2D or 3D rendered images of the object.

[0005] A need exists for improved systems that provide real time navigation in ultrasound volumetric data.

[0006] The invention is defined in independent claim 1.

[0007] In one embodiment of the invention, an ultrasound system is provided that includes a probe having a 2D array of transducers for acquiring ultrasound information along a plurality of scan lines through an object in real time. The scan lines are arranged to define volumetric data corresponding to a volume of interest (VOI) in a subject or patient. One such VOI may include the human heart or some portion of the human heart. The system includes a beamformer configured with scan parameter values that define the scan lines. An image buffer stores multiple data volumes acquired over time that are successively retrieved and processed by a display processor. The display processor accesses the data volumes stored in the image buffer successively to control generation of at least one of 2D and 3D renderings based on display parameters, wherein the display processor obtains from the image buffer a first data volume defined based on first scan parameter values, while the probe acquires ultrasound information for a second data volume that is entered into the image buffer. The second data volume is defined based on second scan parameter values. A navigation view presents in real time the renderings generated by the display processor with their corresponding 3D orientation. A navigator is provided that controls the display of the navigation view in real time such that, as the user adjusts a display parameter value to change a view plane, images presented in the navigation view are updated to reflect the view plane. A user interface is provided for adjusting the scan and display parameter values.

[0008] The invention will now be described in greater detail, by way of example, with reference to the drawings, in which:-

Figure 1 is a block diagram of an ultrasound system formed in accordance with an embodiment of the present invention.

Figure 2 is a flowchart of an exemplary method supporting real time navigation of 2D and 3D rendering views produced and displayed from acquired volumetric data. Said method doesn't form part of the present invention.

Figure 3 is an illustration of a navigation view with a view plane looking into a volume from the left that may be produced by the system of Figure 1.

Figure 4 is an illustration of a navigation view with a view plane looking into the volume of Figure 3 from the top.

Figure 5 is an illustration of the navigation view of Figure 4 with the view plane translated downwards.

Figure 6 is an illustration showing a volume obtained with a selected width and elevation, the width and elevation selected through a user interface of the system of Figure 1.

Figure 7 is an illustration showing a changed volume obtained by changing the width and elevation for the volume of Figure 6.

Figure 8 is an illustration of a navigation view of a heart as seen from a view plane selected by the user of the system of Figure 1.

[0009] Figure 1 is a block diagram of an ultrasound system 100 formed in accordance with an embodiment of the present invention. The ultrasound system 100 is configurable to acquire volumetric data corresponding to a volume of interest (VOI) in a subject or patient. One such VOI may include the human heart or some portion of the human heart. The ultrasound system 100 is configurable to acquire 3-dimensional (3D) volumes of data, each volume defined by an azimuth angle and elevation angle. The ultrasound system 100 includes a 2-dimensional (2D) array/matrix probe 102 that under the guidance of a beamformer 104 scans the VOI and acquires volumes of data at a rate of 15-30 volumes/sec, depending on the size of the volume (azimuth angle and elevation angle). The probe 102 receives backscattered echoes from the scanned object within the VOI and generates electrical receive signals that are combined in the beamformer 104 to form each beam/line within each scan plan. Multiple scan plans (differentiated by their elevation angle) combine to form a volume. The beamformer 104 outputs the beam information to an RF processor 106 that converts the beam information into ultrasound imaging data, e.g. B-mode information. The B-mode information generated from the RF processor 106 is stored in an

image buffer 108. The image buffer 108 is a ring buffer that stores each acquired volume at a rate depending upon the size of each volume. Each volume in the image buffer 108 is given a time stamp.

[0010] While B-mode information is stored in the image buffer 108, previously stored B-mode information is retrieved and made available, a volume at a time, to a display processor 110 and a navigator 114. The display processor 110 and the navigator 114 receive the same set of inputs, e.g. a set of scan parameters 116, a set of display parameters 118, and volume data from the image buffer 108 for processing. The image buffer 108 is a ring buffer in that the buffer 108 wraps around on itself. When the last storage location in the buffer 108 is reached, the beginning location in the buffer 108 is next addressed. Volumetric information is retrieved from the buffer 108 by the display processor 110 and the navigator 114 at a rate that prevents overwriting of information in the image buffer 108.

[0011] The display processor 110 processes the volume information retrieved from the image buffer 108 to form a rendering such as, for example, a volume rendering or a slice (cut) plane rendering, that is displayed in a rendering view 122 of a computer display 112. The rendering view 122 displays an image of the scanned object as would be seen from a desired orientation or view plane (direction of view) as determined by the display parameters 118. The orientation or view plane from which the rendering view 122 is formed and displayed may be displayed to the user by a navigation view 124 in the computer display 112. The navigator 114 generates and controls the navigation view 124 that is displayed on the computer display 112. The navigation view 124 may show a high level view of the scanned object and the orientation or direction of view of the scanned object by positioning the scanned object with respect to a set of planes or slices, such as a set of orthogonal planes or slices that form a Cartesian reference system.

[0012] The user through a user interface 120 may change the scan parameters 116 and/or the display parameters 118. The navigator 114 controls the orientation shown in the navigation view 124 based on the values of the display parameters 118. When changing the navigation view 124 by changing the display parameters 118, the display of the rendering view 122 is correspondingly changed to show the scanned object as formed and seen from the new view direction and/or orientation. Thus, the user may navigate and change the direction of view and/or orientation of the scanned object as is displayed in the navigation view 124, and in so doing, change the view of the scanned object that is displayed in the rendering view 122. The display of the scanned object shown in rendering view 122 is aligned to agree and correspond with the new view orientation that is shown in the navigation view 124. Direction of view (the navigation view 124) may be changed while new volume data is being acquired and stored in the image buffer 108. The user is able to navigate in real time the view or perspective being

displayed of the scanned object while the object is being scanned. The lag time to see changes made in the display parameters 118 (changes in the viewing direction and/or orientation) update the rendering view 122 and the navigation view 124 depends on the time required to generate new renderings. Unlike changing the scan parameters 116, changing the display parameters 118 does not affect the configuration of the beamformer 104.

[0013] Figure 2 is a flowchart 200 of an exemplary method supporting real time navigation of 2D and 3D rendering views 122 produced and displayed in the computer display 112 from acquired volumetric data. At 202, a plurality of scan planes is defined based on values assigned to the scan parameters 116. The scan parameters 116 include such variables as, for example, scan depth, width (azimuth angle), elevation angle, number of beams (beam density) in elevation and in azimuth, number of samples/beam, and mode. The user may define the values for the scan parameters 116 through the user interface 120, such as through the use of a keyboard, trackball, and/or mouse, and may update the scan parameters 116 in real time during the ultrasound scanning. New scan parameter values are provided to the display processor 110 and the navigator 114. The lag time for seeing the effect of having changed the values of the scan parameters 116 is from 1 to 2 seconds, time being needed to configure the beamformer 104 with the new scan parameters 116.

[0014] At 204, ultrasound information is acquired by utilizing a probe with a 2D array of transducers to collect scan information along a plurality of scan plans through a scanned object. The scanning is performed in real time in that no manual repositioning of the probe is needed in order to acquire all the scan planes that form a data volume. Each scan plan of the volume is differentiated from another by the elevation angle of the beam lines producing the scan plan. The width of the scan plan is determined by an azimuth angle. A volume of scan data may be produced by varying the elevation angle of the scan to generate a plurality of scan planes through the scanned object at different elevations.

[0015] At 206, multiple data volumes are successively stored as acquired over time in the image buffer 108. As related for Figure 1, the image buffer 108 is a ring buffer with data volumes being extracted and used by the display processor 110 and the navigator 114 while data volumes are being stored in the image buffer 108.

[0016] At 208, the 2D or 3D rendering view 122 is presented in the computer display 112 as formed by the display processor 110 based on the scanned volume, the scan parameters 116, and the display parameters 118. At 210 the user may adjust the scan parameters 116 to obtain a wider or narrower scan of the scanned object, or to obtain a scan with a greater density of beams/lines in a scan plane or the elevation (number of scan planes/per volume).

[0017] At 210, the user adjusts the scan parameters 116 and, as the user makes adjustments, the effects of

the adjustments as displayed in the rendering view 122 are presented 208 in the computer display 112. The effects of the adjustments to the scan parameters 116 may be viewed in about 1 or 2 seconds from having entered the adjustments.. The time of 1 or 2 seconds may be needed in order to reconfigure the beamformer 104 with the new scan parameters 116, acquire and store new volume data in the image buffer 108, retrieve and process the new volume data from the image buffer 108 by the display processor 110, and present the updated rendering view 122 in the computer display 112. When the user is satisfied with the size and quality of display of the scanned object in the rendering view 122, the user may want to view the scanned object from a different direction and/or orientation.

[0018] At 212, data volumes are successively accessed from the image buffer 108, and with the current valuing of the scan parameters 116 and the display parameters 118, the rendering view 122 and the navigation view 124 are displayed in the computer display 112. The navigator 114 uses the display parameters 118 to define the orientation or direction of view (view plane) and to display the view plane as part of the navigation view 124 in the computer display 112. The user may adjust the display parameters 118 through the user interface 120 similarly to how the scan parameters 116 are adjusted. Examples of display parameters may include view direction, rotation translation, tilt, zoom factor, and number of images viewed. Both the display processor 110 and the navigator 114 read the display parameters 118. The navigator 114 produces a view plane or angle of view with a view of the scanned object in the navigation view 124. The rendering view 122 may be an enlarged view of the scanned object in comparison to the scanned object shown in the navigation view 124. The rendering view 122 and the navigation view 124 may each be displayed in a quadrant of the computer display 112.

[0019] Real time navigation is obtained by successively accessing data volumes stored in the image buffer 108 and scan parameter values stored in 116 and presenting at least one of 2D and 3D images based on display parameters 118, wherein each image that is displayed is defined based on separate display parameter values stored in display parameters 118.

[0020] Figure 3 is an illustration of a navigation view 300 with a view plane 310 looking into a volume 308 from the left that may be produced by the system 100 of Figure 1. The navigation view 300 shows an image of a heart valve 306 generated as seen from viewing into a volume 308 from the left. The view plane 310, is shown as a table top with four arrows for legs, and indicates to the user that the image of the heart valve 306 is produced by looking perpendicularly through the view plane 310 (perpendicularly through the table top) into the volume 308. The image of the heart valve 306 may be formed by use of various techniques, such as slice (cut plane) imaging, surface rendering, and the like. The user may change the orientation of the view plane 310 with respect to the

volume 308 by rotating and/or translating the view plane 310. For example, the view plane 310 may be reoriented about the volume 308 to obtain a view plane 312 and view of the heart valve 306 as shown in Figure 4.

[0021] Figure 4 is an illustration of a navigation view 302 with a view plane 312 looking into the volume 308 from the top. A translation and/or rotation of the view plane 310 of Figure 3 obtains the view plane 312 of Figure 4. Shown in Figure 4 is an object 314 between the view plane 312 and the heart valve 306. The view from the view plane 312 includes the object 314 which may obstruct the view of a portion of the heart valve 306. The generated image of the heart valve 306 has the object 314 obstructing the view of the heart valve 306. The obstructed view may be resolved by translating the view plane 312 downward as shown in Figure 5.

[0022] Figure 5 is an illustration of the navigation view 302 of Figure 4 with the view plane 312 translated downward. The view plane 312 of navigation view 302 has been lowered down (translated downward) to be closer to the heart valve 306 in Figure 5. The new view plane 316 is positioned below the obstructing object 314 to result in an image of the heart valve 306 that is no longer obstructed by the object 314. By translating the view plane 312 downward to obtain the view plane 316, the user has eliminated use of the volumetric scan data that contains the obstructing object 314 in forming the view or image of the heart valve 306. The user may change the values of display parameters 118 through the use of the user interface 120 of Figure 1 to reorient the view plane 312. Reorientation may result in a view of the heart valve 306 from a different angle and/or without obstructing objects within the view.

[0023] Figure 6 is an illustration 400 showing a volume 401 obtained with a selected width 410 (azimuth angle θ) and elevation 408 (elevation angle ϕ), the width 410 and elevation 408 selected by the user through the user interface 120 of the system 100 of Figure 1. The volume 401 is determined from the width 410 (the azimuth angle θ) of a scan slice 416 and the elevation 408 (the elevation angle ϕ) for the scan slice 416. Figure 6 shows a view plane 404 through which an image of a heart valve 406 is defined and displayed. When observing the display of the heart valve 406, the user or sonographer may desire to display more of the heart valve 406 or more area surrounding the heart valve 406, but with the view remaining unchanged. A larger view of the heart valve 406 may be obtained as shown in Figure 7.

[0024] Figure 7 is an illustration 402 showing a changed volume 403 obtained by changing the width 410 and elevation 408 for the volume 401 of Figure 6. In Figure 7, a shortened width 414 and increased elevation 412 through which scan slices 416 are obtained is specified by the user to obtain the changed volume 403. Without changing the view plane 404 of Figure 6, a larger view of the heart valve 406 is obtained by increasing the volume 403 of the scan.

[0025] Figure 8 is an illustration of a navigation view

500 of a heart 506 as seen from a view plane 502 selected by the user of the system 100 of Figure 1. The heart 506 is shown with an aortic structure 510 facing the view plane 502. The image of the heart 506 in the navigation view 500 may be generated as a surface rendering. In an alternative embodiment, the image shown of the heart 506 may not be a generic surface model, but instead may be a calibrated model of a heart.

[0026] The system 100 may generate a model of a heart constructed from a plurality of polygons and position the heart model in the location of the heart 506. To be useful, the heart model is scaled based on data from the patient. Data may be manually measured or automatically determined to scale the size of the heart model based on actual size of the patient's heart. For example, the actual size of the patient's heart may be determined based on three landmarks in data (e.g. two points on the mitral ring and the aortic output) and apex. The generated heart model is positioned and oriented within the volume 508 according to the landmarks in the volume data. Thus, the navigation view 500 may show a heart 506 that is a calibrated scale model of the patient's heart positioned and oriented correctly within the volume 508. Corresponding to the view plane 502 of the navigation view 500, a rendering view (not shown in the figure) may show 2D or 3D images derived from the ultrasound scan data. The view plane 502 may intersect the heart model.

[0027] Exemplary embodiments of diagnostic ultrasound systems are described above in detail. The systems are not limited to the specific embodiments described herein, but rather, components of each system may be utilized independently and separately from other components described herein. Each system component can also be used in combination with other system components.

Claims

1. An ultrasound system (100), comprising:

a probe (102) having a 2D array of transducers adapted to acquire (204) ultrasound information along a plurality of scan lines through an object (314) in real time, said scan lines being arranged to define (202) data volumes (308, 401, 508) within the object (314);
 a beamformer (104) connected to the probe (102) having scan parameters (116) that define (202) said scan lines, said scan parameters (116) having parameter values;
 an image buffer (108) adapted to be fed with an store (206) multiple data volumes (308, 401, 508) successively acquired (204) over time from the probe (102);
 a display processor (110) adapted to access (212) said data volumes (308, 401, 508) stored (206) in said image buffer (108) successively to

control generation of at least one of 2D and 3D renderings (122) based on display parameters (118), wherein said display processor (110) adapted to obtain 204 from said image buffer (108) a first data volume (308, 401, 508) defined (202) based on first scan parameter values and said probe (102) is adapted to acquire (204) ultrasound information for a second data volume (308, 401, 508), said second data volume (308, 401, 508) being defined (202) based on second scan parameter values, the image buffer (108) being adapted to be entered with the second data volume (308, 401, 508) while said display processor (110) obtains the first volume data (308, 401, 508);

a navigation view (124) adapted to present (208) in real time the at least one of 2D and 3D renderings (122) generated by said display processor (110) with their corresponding 3D orientation;

a user interface (120) for adjusting (210) said scan and display parameter values

and a navigator (114) adapted to control display (112) of said navigation view (124, 300, 302, 500) in real time such that, as the user adjusts (210) through said user interface (120) a display value to change a view plane, images (310, 312, 316, 404, 502), presented (208) in said navigation view (124, 300, 302, 500) are updated to reflect said view plane (310, 312, 316, 404, 502).

2. The ultrasound system (100) of Claim 1, wherein said user interface (120) is adapted to permit a user to adjust (210) said scan parameters (116) from said first parameter values to said second parameter values while viewing said at least one of 2D and 3D renderings (122) based on volume data being acquired (204) in real time.

3. The ultrasound system (100) of Claim 1, wherein said image buffer (108) is adapted simultaneously store (206) said first and second data volumes

4. The ultrasound system (100) of Claim 1, wherein said image buffer (108) is adapted to be substantially simultaneously accessed (212) by said display processor (110) to read said data volumes (308, 401, 508) from said image buffer (108) and by said beamformer (104) to write said data volumes (308, 401, 508) to said image buffer (108); and store (206) a time stamp with each of said data volumes (308, 401, 508), said time stamp identifying a time at which each of data volume (308, 401, 508) was acquired (204).

5. The ultrasound system (100) of Claim 1, wherein said display (112) is adapted to present (208) at least

one of volume rendered images (122), surface rendered images (122) and cut plane images (310, 312, 316, 404, 502).

6. The ultrasound system (100) of Claim 1, wherein the navigator (114) is adapted to control the display (112) of the navigation view (124, 300, 302, 500) to indicate at least one of view planes (310, 312, 316, 404, 502), object (314) models and landmarks relative to said data volumes (308, 401, 508), said navigation view (124, 300, 302, 500) being defined (202) based on said data volumes and scan and display parameter values. 5
7. The ultrasound system (100) of Claim 1, wherein said probe (102) is adapted to continue to acquire (204) new data volumes (308, 401, 508) as display parameters values for said display parameters (118) are changed. 10
8. The ultrasound system (100) of Claim 1, wherein a lag time after changing display parameter values before displaying (208) updated images based on new display parameter values is no more than ¼ second. 15
9. The ultrasound system (100) of Claim 1, wherein a lag time after changing scan parameter values before displaying (208) updated images based on new scan parameter values is no more than 2 seconds. 20

Patentansprüche

1. Ultraschallsystem (100), aufweisend:

eine Sonde (102) mit einer 2D-Anordnung von Wandlern, die dafür angepasst sind, Ultraschallinformation entlang mehreren Scanlinien durch ein Objekt (314) in Echtzeit zu erfassen (204), wobei die Scanlinien so angeordnet sind, dass sie Datenvolumina (308, 401, 508) in dem Objekt (314) definieren (202);
einen mit der Sonde (102) verbundenen Strahlformer (104) mit Scanparametern (116), die die Scanlinien definieren (202), wobei die Scanparameter (116) Parameterwerte haben;
einen Bildpuffer (108), der dafür angepasst ist, mit mehreren sukzessiv mit der Zeit von der Sonde (102) erfassten (204) Datenvolumina (308, 401, 508) gespeist zu werden und diese zu speichern (206);
einen Anzeigeprozessor (110), der dafür angepasst ist, auf die in dem Bildpuffer (108) gespeicherten (206) Datenvolumina (308, 401, 508) sukzessiv zuzugreifen (212), um die Erzeugung von wenigstens einer von 2D- und 3D-Renderings (Wiedergabedarstellungen) (122) auf der Basis von Anzeigeparametern (118) zu steuern, 50

wobei der Anzeigeprozessor (110) dafür angepasst ist, aus dem Bildpuffer (108) ein auf der Basis der ersten Scanparameterwerte definiertes (202) erstes Datenvolumen (308, 401, 508) zu erhalten (204), und die Sonde (102) dafür angepasst ist, Ultraschallinformation für ein zweites Datenvolumen (308, 401, 508) zu erfassen, wobei das zweite Datenvolumen (308, 401, 508) auf der Basis von zweiten Scanparameterwerten definiert ist (202), wobei der Bildpuffer (108) dafür angepasst ist, dass das zweite Datenvolumen (308, 401, 508) darin eingegeben wird, während der Anzeigeprozessor (110) die ersten Volumendaten (308, 401, 508) erhält;
eine Navigationsansicht (124), die dafür angepasst ist, in Echtzeit wenigstens eine von den von dem Anzeigeprozessor (110) erzeugten 2D- und 3D-Renderings (122) mit ihrer entsprechenden 3D-Ausrichtung zu präsentieren (208);
eine Benutzerschnittstelle (102) zum Anpassen (210) der Scan- und Anzeigeparameterwerte; und
einen Navigator (114), der dafür angepasst ist, die Anzeige (112) der Navigationsansicht (124, 300, 302, 500) in Echtzeit dergestalt zu steuern, dass, sobald der Benutzer (110) über die Benutzerschnittstelle (102) einen Anzeigeparameterwert anpasst, um eine Ansichtsebene zu ändern, in der Navigationsansicht (124, 300, 302, 500) präsentierte (208) Bilder, (310, 312, 316, 404, 502) aktualisiert werden, um die Ansichtsebene (310, 312, 316, 404, 502) wiederzugeben.

2. Ultraschallsystem (100) nach Anspruch 1, wobei die Benutzerschnittstelle (120) dafür angepasst ist, einem Benutzer eine Anpassung (210) der Scanparameter (116) von den ersten Parameterwerten zu den zweiten Parameterwerten während einer Betrachtung der wenigstens einen von 2D- und 3D-Renderings (122) auf der Basis von in Echtzeit erfassten (204) Volumendaten zu ermöglichen. 35
3. Ultraschallsystem (100) nach Anspruch 1, wobei der Bildpuffer (108) dafür angepasst ist, simultan die ersten und zweiten Datenvolumina zu speichern (206). 40
4. Ultraschallsystem (100) nach Anspruch 1, wobei der Bildpuffer (108) dafür angepasst ist, dass auf ihn im Wesentlichen gleichzeitig durch den Anzeigeprozessor (110) zum Auslesen der Datenvolumina (308, 401, 508) aus dem Bildpuffer (108), und durch den Strahlformer (104) zum Schreiben der Datenvolumina (308, 401, 508) in den Bildpuffer (108), zugegriffen wird (212); und
einen Zeitstempel mit jedem der Datenvolumina (308, 401, 508) zu speichern (206), wobei der Zeitstempel einen Zeitpunkt identifiziert, an welchem je- 55

des von den Datenvolumina (308, 401, 508) erfasst wurde (204).

5. Ultraschallsystem (100) nach Anspruch 1, wobei die Anzeige (112) dafür angepasst ist, wenigstens eines von Volumen-gerenderten Bildern (122), Oberflächen-gerenderten Bildern (122) und Schnittebenen-Bildern (310, 312, 316, 404, 502) zu präsentieren (208). 5
6. Ultraschallsystem (100) nach Anspruch 1, wobei der Navigator (114) dafür angepasst ist, die Anzeige (112) der Navigationsansicht (124, 300, 302, 500) zu steuern, um wenigstens eine von Betrachtungsebenen (310, 312, 316, 404, 502), Modelle eines Objektes (314) und Markierungen bezüglich der Datenvolumina (308, 401, 508) anzuzeigen, wobei die Navigationsansicht (124, 300, 302, 500) auf der Basis der Datenvolumina und Scan- und Anzeigeparameterwerte definiert (202) ist. 10
7. Ultraschallsystem (100) nach Anspruch 1, wobei die Sonde (102) dafür angepasst ist, mit der Erfassung (204) neuer Datenvolumina (308, 401, 508) fortzufahren, während Anzeigeparameterwerte für die Anzeige (118) geändert werden. 15
8. Ultraschallsystem (100) nach Anspruch 1, wobei eine Verzögerungszeit nach einer Änderung von Anzeigeparameterwerten vor einer Anzeige (208) aktualisierter Bilder auf der Basis neuer Anzeigeparameterwerte nicht mehr als 1/4 Sekunden beträgt. 20
9. Ultraschallsystem (100) nach Anspruch 1, wobei eine Verzögerungszeit nach Änderung von Scanparameterwerten vor der Darstellung (208) aktualisierter Bilder auf der Basis neuer Scanparameterwerte nicht mehr als 2 Sekunden beträgt. 25

Revendications

1. Système ultrasonore (100), comprenant :

une sonde (102) comprenant un groupement 2D de transducteurs, conçue pour acquérir des informations ultrasonores le long d'une pluralité de lignes de balayage à travers un objet (314) en temps réel, lesdites lignes de balayage étant agencées pour définir (202) des volumes de données (308, 401, 508) à l'intérieur de l'objet (314) ;
un dispositif de formation de faisceau (104) connecté à la sonde (102), ayant des paramètres de balayage (116) qui définissent (202) lesdites lignes de balayage, lesdits paramètres de balayage (116) ayant des valeurs de paramètres ;
un tampon d'image (108) conçu pour recevoir 45

et stocker (206) de multiples volumes de données (308, 401, 508) successivement acquis (204) au cours du temps par la sonde (102) ;
un processeur d'affichage (110) conçu pour accéder (212) auxdits volumes de données (308, 401, 508) stockés (206) dans ledit tampon d'image (108) successivement afin de commander la génération d'au moins un rendu parmi des rendus 2D et 3D (122) sur la base de paramètres d'affichage (118), ledit processeur d'affichage (110) étant conçu pour obtenir (204) à partir dudit tampon d'image (108) un premier volume de données (308, 401, 508) défini (202) sur la base de premières valeurs de paramètres de balayage et ladite sonde (102) étant conçue pour acquérir (204) des informations ultrasonores pour un second volume de données (308, 401, 508), ledit second volume de données (308, 401, 508) étant défini (202) sur la base de secondes valeurs de paramètres de balayage, le tampon d'image (108) étant conçu pour recevoir le second volume de données (308, 401, 508) pendant que ledit processeur d'affichage (110) obtient les données du premier volume (308, 401, 508) ;
une vue de navigation (124) conçue pour présenter (208) en temps réel l'au moins un rendu parmi des rendus 2D et 3D (122) généré par ledit processeur d'affichage (110) avec son orientation 3D correspondante ;
une interface utilisateur (120) pour ajuster (210) lesdites valeurs de paramètres de balayage et d'affichage ; et
un navigateur (114) conçu pour commander l'affichage (112) de ladite vue de navigation (124, 300, 302, 500) en temps réel de telle manière que, à mesure que l'utilisateur ajuste (210), par l'intermédiaire de ladite interface utilisateur (120), une valeur de paramètre d'affichage afin de changer un plan de vue, des images (310, 312, 316, 404, 502) présentées (208) dans ladite vue de navigation (124, 300, 302, 500) soient mises à jour pour refléter ledit plan de vue (310, 312, 316, 404, 502). 40

2. Système ultrasonore (100) selon la revendication 1, dans lequel ladite interface utilisateur (120) est conçue pour permettre à un utilisateur d'ajuster (210) lesdits paramètres de balayage (116), desdites premières valeurs de paramètres auxdites secondes valeurs de paramètres, tout en regardant ledit au moins un rendu parmi des rendus 2D et 3D (122) sur la base de données de volume acquises (204) en temps réel.
3. Système ultrasonore (100) selon la revendication 1, dans lequel ledit tampon d'image (108) est conçu pour simultanément stocker (206) lesdits premier et 55

second volumes de données.

4. Système ultrasonore (100) selon la revendication 1, dans lequel ledit tampon d'image (108) est conçu pour : 5

être sensiblement simultanément accessible (212) par ledit processeur d'affichage (110) pour lire lesdits volumes de données (308, 401, 508) dans ledit tampon d'image (108) et par ledit dispositif de formation de faisceau (104) pour écrire lesdits volumes de données (308, 401, 508) dans ledit tampon d'image (108) ; et 10

stocker (206) une estampille temporelle avec chacun desdits volumes de données (308, 401, 508), ladite estampille temporelle identifiant un instant auquel chacun desdits volumes de données (308, 401, 508) a été acquis (204). 15

5. Système ultrasonore (100) selon la revendication 1, dans lequel ledit dispositif d'affichage (112) est conçu pour présenter (208) des images d'au moins un type parmi des images de rendu de volume (122), des images de rendu de surface (122) et des images de plan de coupe (310, 312, 316, 404, 502). 20
25

6. Système ultrasonore (100) selon la revendication 1, dans lequel le navigateur (114) est conçu pour commander l'affichage (112) de la vue de navigation (124, 300, 302, 500) afin d'indiquer au moins un élément parmi des plans de vue (310, 312, 316, 404, 502), des modèles de l'objet (314) et des repères relatifs auxdits volumes de données (308, 401, 508), ladite vue de navigation (124, 300, 302, 500) étant définie (202) sur la base desdits volumes de données et de valeurs de paramètres de balayage et d'affichage. 30
35

7. Système ultrasonore (100) selon la revendication 1, dans lequel ladite sonde (102) est conçue pour continuer à acquérir (204) de nouveaux volumes de données (308, 401, 508) à mesure que des valeurs de paramètres d'affichage pour lesdits paramètres d'affichage (118) sont modifiées. 40
45

8. Système ultrasonore (100) selon la revendication 1, dans lequel un temps de latence après une modification de valeurs de paramètres d'affichage avant l'affichage (208) d'images mises à jour sur la base de nouvelles valeurs de paramètres d'affichage n'est pas supérieur à ¼ seconde. 50

9. Système ultrasonore (100) selon la revendication 1, dans lequel un temps de latence après une modification de valeurs de paramètres de balayage avant l'affichage (208) d'images mises à jour sur la base de nouvelles valeurs de paramètres de balayage n'est pas supérieur à 2 secondes. 55

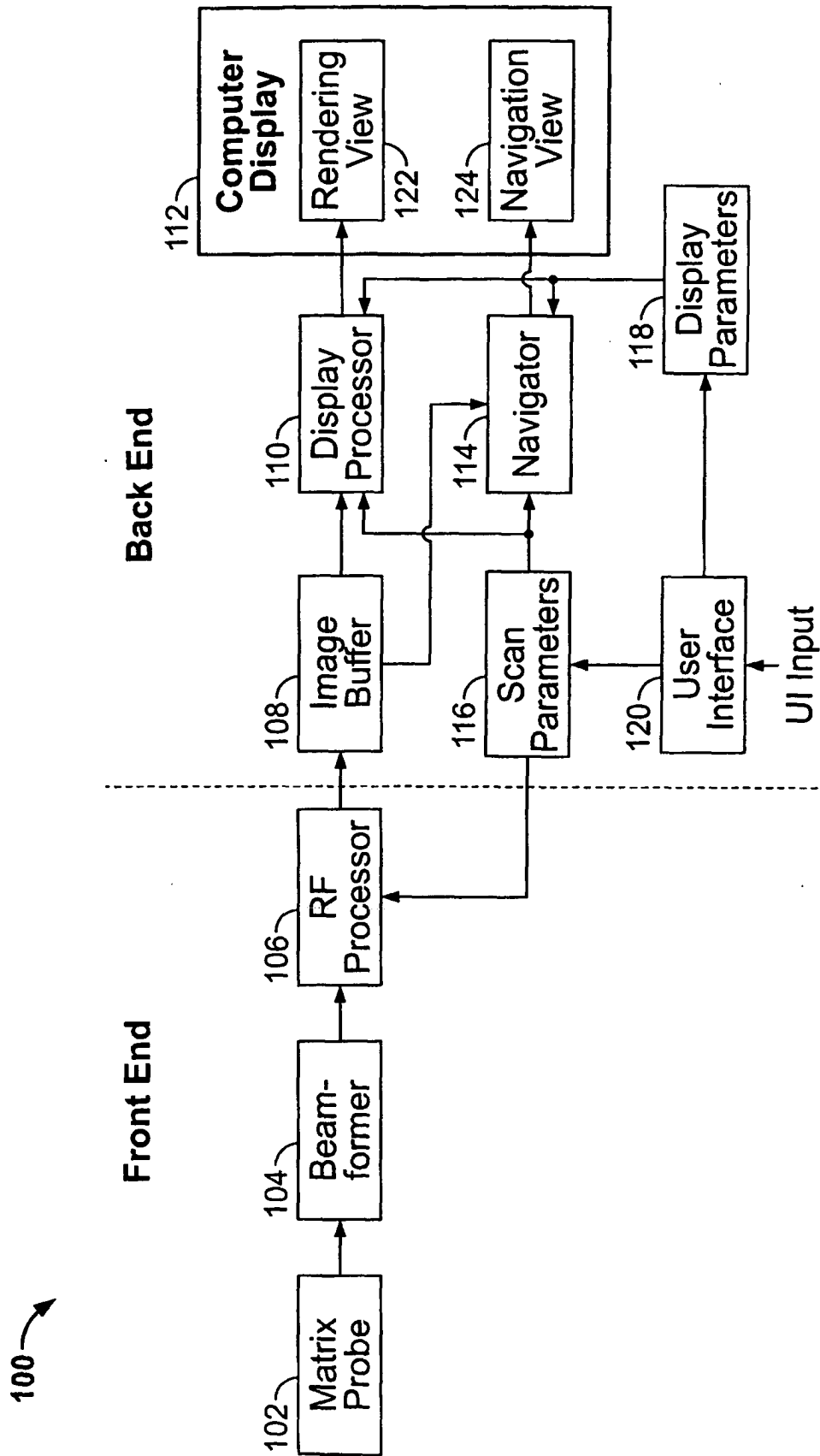


FIG. 1

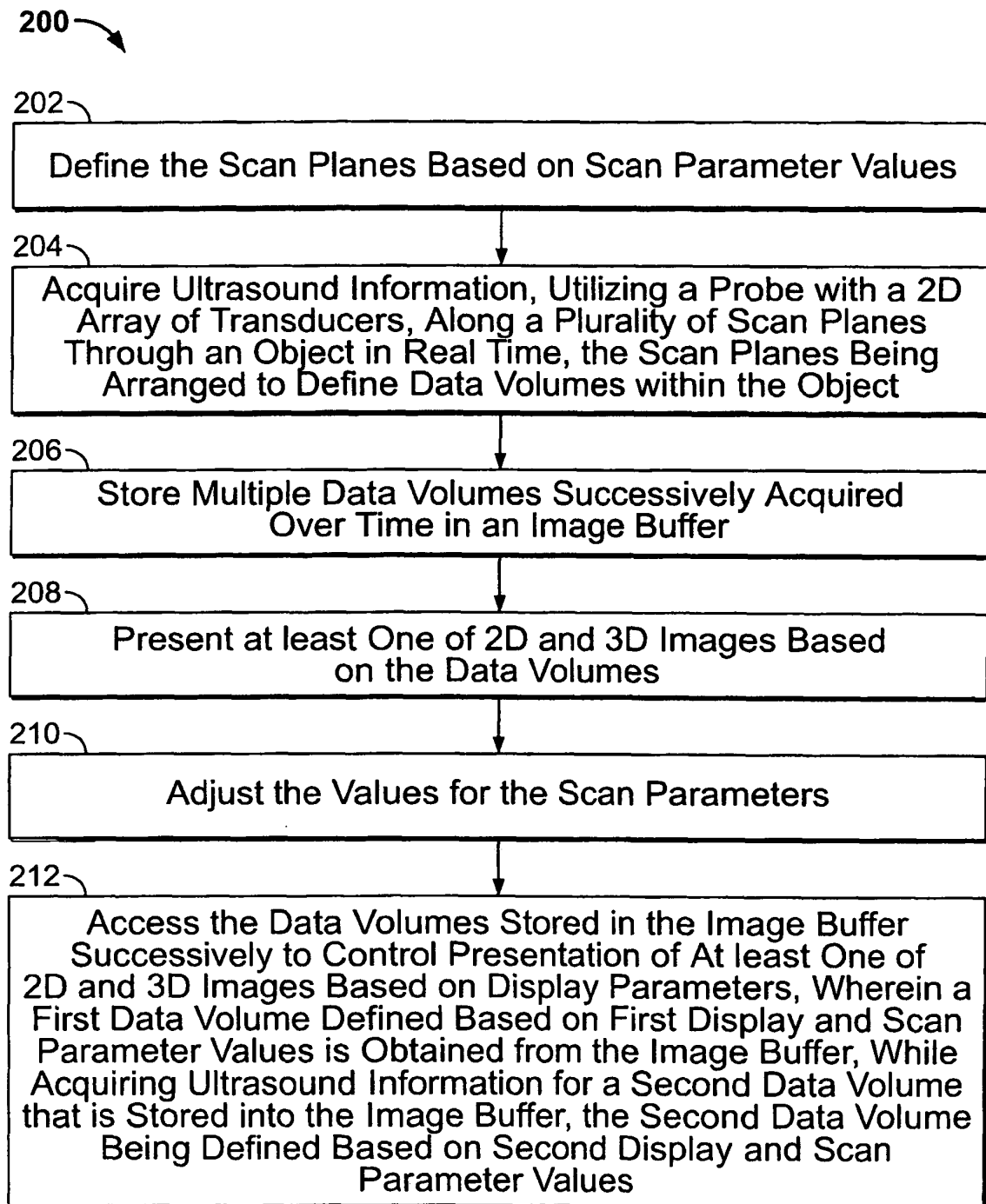


FIG. 2

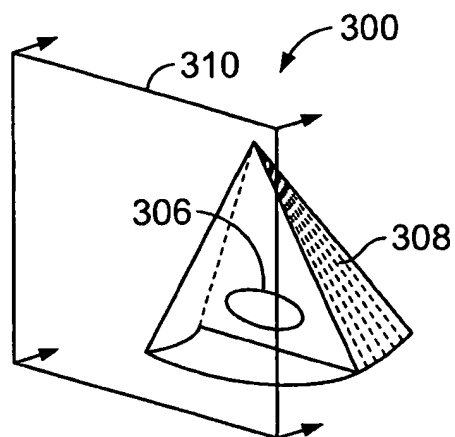


FIG. 3

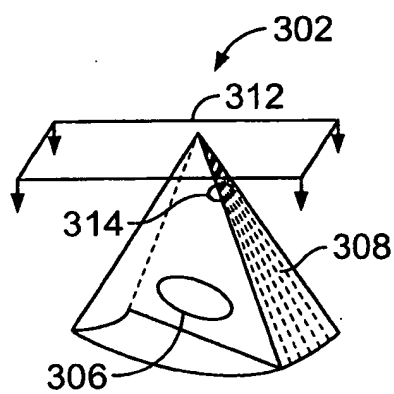


FIG. 4

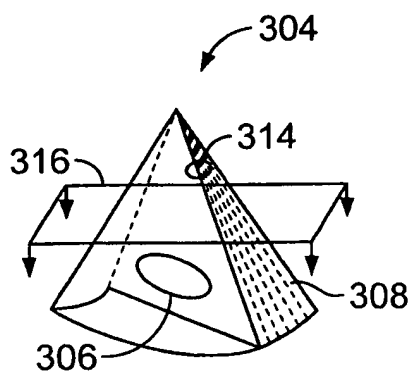


FIG. 5

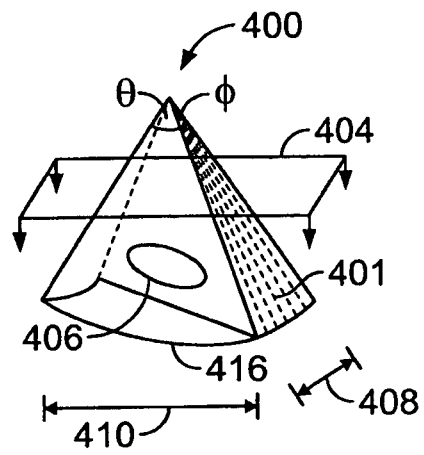


FIG. 6

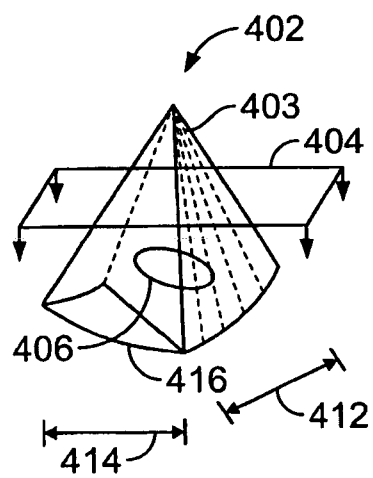


FIG. 7

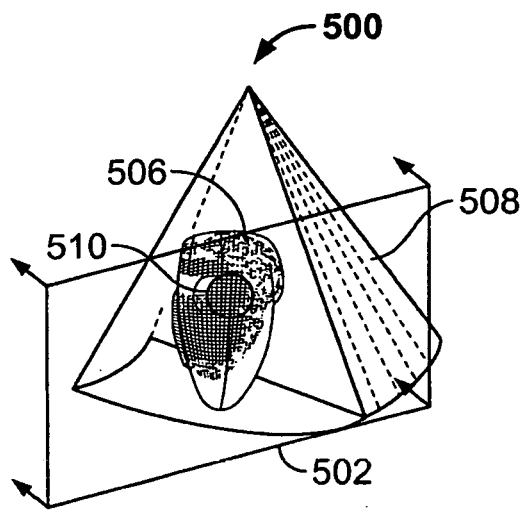


FIG. 8

REFERENCES CITED IN THE DESCRIPTION

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Patent documents cited in the description

- WO 2004029655 A [0003]

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摘要(译)

在一个实施例中，提供了一种超声系统（100），其包括具有2D换能器阵列的探头（102），用于沿着通过物体的多个扫描线实时采集超声信息。扫描线被布置成限定对应于受试者或患者中的感兴趣体积（VOI）的体积数据。一种这样的VOI可以包括人的心脏或人的心脏的某些部分。该系统包括波束形成器（104），其配置有定义扫描线的扫描参数值。图像缓冲器（108）存储随时间获取的多个数据量，这些数据量由显示处理器（110）连续检索和处理。显示处理器（110）连续访问存储在图像缓冲器（108）中的数据量，以基于显示参数（118）控制2D和3D渲染（122）中的至少一个的生成，其中显示处理器（110）获得从图像缓冲器（108），基于第一扫描参数定义的第一数据量当探测器（102）获取进入图像缓冲器（108）的第二数据量的超声信息时，值。基于第二扫描参数值定义的第二数据量。导航视图（124）实时呈现由显示处理器（110）生成的渲染（122）及其对应的3D方向。提供导航器，其实时控制导航视图（124）的显示，使得当用户调整（210）显示参数值以改变视平面时，导航视图（124）中呈现的图像（122）更新以反映视图平面。提供用户界面（120）用于调整扫描和显示参数值。

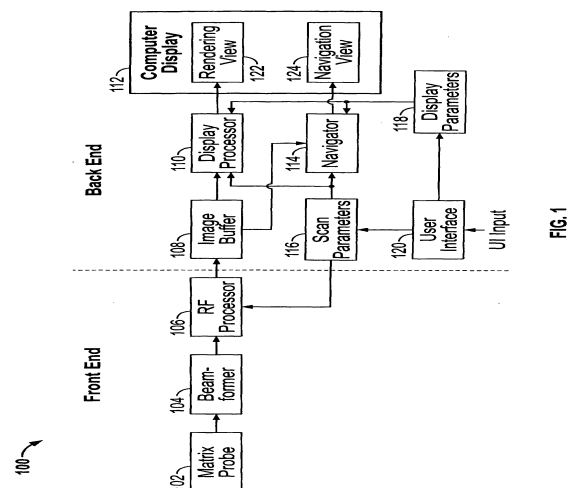


FIG. 1