

(19)



(11)

EP 2 320 802 B1

(12)

## EUROPEAN PATENT SPECIFICATION

(45) Date of publication and mention  
of the grant of the patent:  
**01.08.2018 Bulletin 2018/31**

(51) Int Cl.:  
**A61B 8/00 (2006.01)** **G01N 29/24 (2006.01)**  
**G01N 29/36 (2006.01)** **G01S 15/89 (2006.01)**  
**G01S 7/52 (2006.01)**

(21) Application number: **09805593.2**

(86) International application number:  
**PCT/US2009/053096**

(22) Date of filing: **07.08.2009**

(87) International publication number:  
**WO 2010/017445 (11.02.2010 Gazette 2010/06)**

---

**(54) IMAGING WITH MULTIPLE APERTURE MEDICAL ULTRASOUND AND SYNCHRONIZATION OF ADD-ON SYSTEMS**

BILDGEBUNG MIT MEDIZINISCHEM MULTIAPERATUR-ULTRASCHALL UND  
SYNCHRONISIERUNG VON ADD-ON-SYSTEMEN

IMAGERIE ULTRASONORE MÉDICALE À OUVERTURES MULTIPLES ET SYNCHRONISATION  
DE SYSTÈMES COMPLÉMENTAIRES

---

(84) Designated Contracting States:  
**AT BE BG CH CY CZ DE DK EE ES FI FR GB GR  
HR HU IE IS IT LI LT LU LV MC MK MT NL NO PL  
PT RO SE SI SK SM TR**

(30) Priority: **08.08.2008 US 87571 P**  
**14.04.2009 US 169264 P**

(43) Date of publication of application:  
**18.05.2011 Bulletin 2011/20**

(73) Proprietor: **Maui Imaging, Inc.**  
**Sunnyvale, CA 94089 (US)**

(72) Inventors:  

- SPECHT, Donald, F.**  
**Sunnyvale, CA 94089 (US)**
- BREWER, Kenneth, D.**  
**Sunnyvale, CA 94089 (US)**

(74) Representative: **Potter Clarkson LLP**  
**The Belgrave Centre**  
**Talbot Street**  
**Nottingham NG1 5GG (GB)**

(56) References cited:  
**US-A- 5 355 888** **US-A1- 2003 028 111**  
**US-A1- 2004 138 565** **US-A1- 2006 270 934**  
**US-A1- 2007 055 155** **US-A1- 2008 103 393**

EP 2 320 802 B1

---

Note: Within nine months of the publication of the mention of the grant of the European patent in the European Patent Bulletin, any person may give notice to the European Patent Office of opposition to that patent, in accordance with the Implementing Regulations. Notice of opposition shall not be deemed to have been filed until the opposition fee has been paid. (Art. 99(1) European Patent Convention).

## Description

### FIELD OF THE INVENTION

**[0001]** The present invention relates generally to imaging techniques used in medicine, and more particularly to medical ultrasound, and still more particularly to synchronizing an add-on apparatus to a host ultrasound machine for producing ultrasonic images using multiple apertures.

### BACKGROUND OF THE INVENTION

**[0002]** In conventional ultrasonic imaging, a focused beam of ultrasound energy is transmitted into body tissues to be examined and the returned echoes are detected and plotted to form an image. In echocardiography the beam is usually stepped in increments of angle from a center probe position, and the echoes are plotted along lines representing the paths of the transmitted beams. In abdominal ultrasonography the beam is usually stepped laterally, generating parallel beam paths, and the returned echoes are plotted along parallel lines representing these paths. The following description will relate to the angular scanning technique for echocardiography (commonly referred to as a sector scan). However, the same concept with minor modifications can be implemented in abdominal scanners.

**[0003]** The basic principles of conventional ultrasonic imaging are well described in the first chapter of Echocardiography, by Harvey Feigenbaum (Lippincott Williams & Wilkins, 5th ed., Philadelphia, 1993). These will not be repeated here except as necessary to illustrate the differences between the conventional techniques and the present invention.

**[0004]** It is well known that the average velocity  $v$  of ultrasound in human tissue is about 1540 m/sec, the range in soft tissue being 1440 to 1670 m/sec (see for example P. N. T. Wells, Biomedical Ultrasonics, Academic Press, London, New York, San Francisco, 1977). Therefore, the depth of an impedance discontinuity generating an echo can be estimated as the round-trip time for the echo multiplied by  $v/2$ , and the amplitude is plotted at that depth along a line representing the path of the beam. After this has been done for all echoes along all beam paths, an image is formed. The gaps between the scan lines are typically filled in by interpolation.

**[0005]** In order to insonify the body tissues, a beam formed either by a phased array or a shaped transducer is scanned over the tissues to be examined. Traditionally, the same transducer or array is used to detect the returning echoes. This design configuration lies at the heart of one of the most significant limitations in the use of ultrasonic imaging for medical purposes; namely, poor lateral resolution. Theoretically the lateral resolution could be improved by increasing the aperture of the ultrasonic probe, but the practical problems involved with aperture size increase have kept apertures small and lateral res-

olution poor. Unquestionably, ultrasonic imaging has been very useful even with this limitation, but it could be more effective with better resolution.

**[0006]** In the practice of cardiology, for example, the limitation on single aperture size is dictated by the space between the ribs (the intercostal spaces). For scanners intended for abdominal and other use, the limitation on aperture size is not so obvious, but it is a serious limitation nevertheless. The problem is that it is difficult to keep the elements of a large aperture array in phase because the speed of ultrasound transmission varies with the type of tissue between the probe and the area of interest. According to the book by Wells (cited above), the speed varies up to plus or minus 10% within the soft tissues.

5 When the aperture is kept small, the intervening tissue is, to a first order of approximation, all the same and any variation is ignored. When the size of the aperture is increased to improve the lateral resolution, the additional elements of a phased array may be out of phase and 10 may actually degrade the image rather than improving it.

**[0007]** Instead of replacing the single transmit/receive ultrasound probes that are common in the medical industry, it would be advantageous and cost effective to increase the resolution of these devices with an add-on 15 system. However, adding resolution to existing system would face additional challenges, such as synchronizing an add-on system to the existing host ultrasound machine.

**[0008]** US 5,355,888 discloses an ultrasound imaging 20 system and method. The system includes an active transducer and transmitter for producing a pulse of ultrasonic energy that is steerable in the direction of one or more targets. The active transducer is also coupled to a receiver for receiving an echo of the pulse returned from 25 each target. A second, passive phased-array transducer acts as another receiver and is electronically steerable to receive echoes of the pulse returned from each target. A signal processor processes the echoes received by 30 the receivers from each target to form a composite image of each target.

**[0009]** US 2006/0270934 discloses a method of producing a three dimensional ultrasonic image containing 35 spatial information regarding the placement or operation of an invasive medical device.

40

### SUMMARY OF THE INVENTION

**[0010]** The present invention provides a method of synchronizing an add-on ultrasound system to a host ultrasound probe according to claim 1 and an add-on ultrasound system according to claim 5.

**[0011]** In some embodiments, the add-on ultrasound system can further include a display adapted to display 45 ultrasound images from the processor. The display can be a GUI, for example.

**[0012]** In some embodiments, the add-on ultrasound system can include multiple ultrasound receivers, such as two, three, or even more ultrasound receiver.

**[0013]** The system comprises an algorithm configured to process the received ultrasound pulses to synchronize the add-on system to the host ultrasound probe. The algorithm is adapted to calculate a start of frame of the transmitted ultrasound pulses. The start of frame can be calculated in a variety of ways. In some embodiments, the algorithm can calculate the start of frame by identifying an interval between amplitude peaks that is substantially larger than a pulse repetition interval. In other embodiments, the algorithm can calculate the start of frame by identifying a large change in peak amplitudes during successive scan lines. The large change in peak amplitudes can be from a low to a high or vice versa, for example.

**[0014]** In another embodiment of the invention, the add-on ultrasound system can further comprise a tap that couples the host ultrasound probe to the add-on system. Since the tap has access to all the data from the host probe, the processor of the add-on ultrasound system can be adapted to process data from the tap to synchronize the add-on system to the host ultrasound probe.

**[0015]** The method of synchronizing an add-on ultrasound system to a host ultrasound probe, comprises transmitting ultrasound pulses from the host ultrasound probe, receiving the ultrasound pulses with the add-on ultrasound system, and synchronizing the add-on ultrasound system to the host ultrasound probe with a processor.

**[0016]** In some embodiments, the receiving step further comprises receiving the ultrasound pulses with a receiving probe of the add-on ultrasound system. In other embodiments, the receiving step further comprises receiving the ultrasound pulses with a plurality of receiving probes of the add-on ultrasound system.

**[0017]** The synchronizing step comprises synchronizing the add-on ultrasound system to the host ultrasound probe with the processor based on the transmitted ultrasound pulses. The add-on ultrasound system is synchronized to the host ultrasound probe with an algorithm in the processor.

**[0018]** The algorithm calculates a start of frame of the transmitted pulses. The algorithm can calculate the start of frame by identifying an interval between amplitude peaks that is substantially larger than a pulse repetition interval. In another embodiment, the algorithm can calculate a start of frame by identifying a large change in peak amplitudes during successive scan lines. The peak amplitude changes can be from a low to a high or vice versa, for example.

**[0019]** In some embodiments, the synchronizing step can further comprise synchronizing the add-on ultrasound system to the host ultrasound probe with the processor adapted to process data from a tap that couples the host ultrasound probe to the add-on system.

**[0020]** Another embodiment of the invention is providing ultrasound images to a display from the add-on ultrasound system. The ultrasound pulses can be transmitted into tissue and the ultrasound images can be of the tissue.

## BRIEF DESCRIPTION OF THE DRAWINGS

**[0021]** The novel features of the invention are set forth with particularity in the claims that follow. A better understanding of the features and advantages of the present invention will be obtained by reference to the following detailed description that sets forth illustrative embodiments, in which the principles of the invention are utilized, and the accompanying drawings of which.

**[0022]** In the drawings:

Figs. 1A-1B illustrate add-on systems with single or multiple receive probes to be used with a host ultrasound machine for providing high-resolution ultrasound images.

Fig. 2A is a flowchart showing one embodiment of a sequence of operations that an algorithm in an add-on system may use to synchronize the add-on system to a host ultrasound machine.

Fig. 2B is a plot illustrating the data collected by an add-on ultrasound system.

Figs. 3A-3B illustrate add-on systems with single or multiple receive probes and high impedance taps to be used with a host ultrasound machine for providing high-resolution ultrasound images.

## DETAILED DESCRIPTION OF THE INVENTION

**[0023]** Various embodiments of an ultrasound imaging system are described.

**[0024]** Returned echoes in ultrasonography can be detected by a separate relatively non-directional receiving probe located away from the insonifying probe (e.g., the transmitting probe), and the non-directional receive transducer can be placed in a different acoustic window from the insonifying probe. This non-directional receiving probe can be called an omni-directional or receiving probe because it can be designed to be sensitive to a wide field of view.

**[0025]** If the echoes detected at the receiving probe are stored separately for every pulse from the insonifying transducer, the entire two-dimensional image can be formed from the information received by a single receiving probe. Additional copies of the image can be formed by additional omni-directional probes collecting data from the same set of insonifying pulses.

**[0026]** In one embodiment, an add-on device can be designed as a receive-only device while using an existing ultrasound machine from another manufacturer to act as the insonifying probe and transmit the ultrasound. A design of this type would allow the diagnostic laboratory or medical office to upgrade the B-mode, M-mode, or Doppler resolution of an existing machine without replacing it.

**[0027]** Figs. 1A and 1B illustrate an external add-on system 100 for use with a host ultrasound system 102 and host transmit/receive probe 104 to image tissue 101. In Fig. 1A, the add-on system 100 includes a single receiving probe 106, and in Fig. 1B, the add-on system

includes two receiving probes 106 and 108. The receiving probes 106 and 108 can have receive only capabilities, for example. In other embodiments, the receiving probes 106 and 108 can have transmit and receive capabilities. In other embodiments, the add-on system can include any number of receiving probes, such as three or more receiving probes. As shown in Figs. 1A-1B, the add-on system 100 can further include add-on processor 110 and display 112. Display 112 can be a graphical user interface (GUI), or other appropriate display. Provision is made for time-gain-controls, overall gain, post-processing curves by means of soft buttons, compression levels, and depth of display. Other controls can conveniently be added to the display.

**[0028]** Synchronization of the receiving probes with the host probe is essential for the add-on system described herein. Without synchronizing the receiving probes to the host probe, the add-on system has no way of using the transmitted pulses from the host probe. Methods and algorithms for synchronizing the add-on system 100 to the host system 102 and host probe 104 can be implemented in add-on processor 110, which will be discussed below.

**[0029]** For the ultrasound systems described herein, the transmit functions can be handled by the host ultrasound system and host transmit/receive probe (e.g., a standard ultrasound machine), whereas the receive and display functions can be performed by the add-on system. In order for the add-on system to work with a majority of other manufacturer's current and future ultrasound devices (hereinafter to be referred to as the host system and host probe), it is necessary for the add-on system to deduce most of the properties of the host machine from the host machine or from the received ultrasound signals alone.

**[0030]** The first and most likely strongest pulses of ultrasound received will be directly from the transmit probe. These can easily be distinguished from echoes from deep tissues because they are first and strongest. From these received signals, the pulse repetition interval (PRI), the end of frame gap time, if any, the Total Frame Interval (TFI), and the maximum depth of penetration can be measured. The PRI, which corresponds to a time interval during which a scan line of echo data is collected, is defined as the elapsed time from the beginning of one pulse to the start of the next pulse. The maximum depth of penetration can be determined from the PRI and the known speed of sound in tissue. The actual depth of interest can be selected by a user of the system or can be a default percentage of the maximum depth of penetration.

**[0031]** An essential but more difficult parameter to estimate is the start time of the transmit pulse. Triggering on the first received pulse would be too noisy and would cause objectionable jitter from line to line resulting in degradation of the image. Assuming only that the PRI is a constant for a given set of settings on the host system, the estimated start time for the n'th line is simply the start time for the first line + (n-1)\*(pulse repetition interval). It

remains to estimate the start of the first line of a sector scan.

**[0032]** In Figs. 1A-1B, the timing of the start of the transmit pulse from the host system and host probe can be deduced from the ultrasound pulses transmitted by the host probe and received by one of the receiving probes on either side of the host probe. The first detection of the transmit pulse will be delayed from the start of the transmit pulse because of the distance the transmit pulse has to travel to get to the receiving probe. However, that time delay can be calculated from the probe geometry and subtracted from the time that the pulse is first detected.

**[0033]** The main requirement for the measurement of the start of the transmit pulse is that the PRI be constant for a given set of settings and that a "flywheel" algorithm be used to estimate start of line in fixed repetition intervals. Because PRI is changed only infrequently, the estimation of PRI can be adapted over many scan cycles.

**[0034]** One embodiment of a method of synchronizing an add-on ultrasound system to a host ultrasound probe will now be described. Referring to add-on system 100 of Figs. 1A-1B, host ultrasound probe 104 can transmit ultrasound pulses into tissue 101. The transmitted pulses can be received by the add-on system, such as by receiving probe 106. In some embodiments, such as in Fig. 1B, the add-on system can include a plurality of receiving probes for receiving the transmitted ultrasound signals (e.g., receiving probes 106 and 108). Add-on processor 110 can then synchronize the add-on system to the host ultrasound probe. The processor can use an algorithm or algorithms to synchronize the add-on system to the host probe. When the add-on system is synchronized to the host ultrasound probe, the add-on system can provide high-resolution images of the target tissue being imaged to a display, such as to a GUI.

**[0035]** Fig. 2A shows a flowchart 200 illustrating one embodiment of a flywheel algorithm for determining the timing of the start of a transmit pulse from a host system. Fig. 2B shows a plot 201 illustrating a collection of data collected and used by the algorithm to synchronize an add-on system to a host machine. In Fig. 2B, the data collected can include PRI 2, Amplitude Peaks 4, IFG 6, SOF 8, and TFI 10. It should be understood that the algorithms described herein typically are executed by the add-on processor 110 described above. These algorithms can be programmed into the add-on processor as firmware, software, or hardware, or a combination of all three.

**[0036]** At step 202 of flowchart 200, the add-on system is started (i.e., powered or booted up).

**[0037]** At step 204, the add-on system begins to collect intervals of data. The data can be collected from the host probe, for example, or in some embodiments, from taps to the host probe. The data can be collected for several seconds, such as for approximately 1 to 2 seconds. The data collected will include intervals between peak amplitudes. The interval from one peak amplitude to the next

peak amplitude occurrence corresponds to the PRI (see, for example, PRI 2 of Fig. 2B).

**[0038]** Next, at step 206 of flowchart 200, the PRI is estimated. As described above, the PRI is the elapsed time from the beginning of one pulse to the start of the next pulse. The PRI can be calculated by the add-on processor of the add-on system to be the median of the set of intervals collected during step 204.

**[0039]** Next, at step 208, the number of samples or pulses is counted by an accumulator function of the add-on processor. The accumulator function should be initialized to a value of zero before counting the number of sample times. The accumulator function is a counter of sample times which counts time for a total frame.

**[0040]** Next, at step 210, the algorithm in the add-on processor continues to collect intervals of data and determines a peak signal (see, for example, Amplitude Peaks 4 in Fig. 2B) for each successive set of scan line data.

**[0041]** At step 212, identify Start of Frame (SOF) by one of two methods. In the first embodiment, SOF occurs when the interval between amplitude peaks is substantially larger than the current PRI. This period is designated as the Inter Frame Gap (IFG). If the IFG cannot be distinguished from the PRI, then a second embodiment must be utilized to identify SOF. (see, for example, IFG 6 and PRI 2 in Fig. 2B).

**[0042]** In the second embodiment, the peak amplitude of successive lines are compared. As the host transmit angle sweeps across the frame, a small change in peak amplitude from line to line occurs. When the transmit angle shifts from the end-of-frame to the beginning-of-frame, there is a corresponding large change in peak amplitude. This change is used to identify SOF. See, for example, how the Amplitude Peaks 4 in Fig. 2B slowly change from line to line until a large change at SOF 8. The peak amplitudes can change from a low to a high, as shown in Fig. 2B, or vice versa.

**[0043]** At step 214, the add-on processor determines the total frame interval. The total frame interval is the interval between successive SOF times (in samples). See, for example, TOF 10 in Fig. 2B.

**[0044]** At step 216, the add-on system collects another set of data from.

**[0045]** At step 218, the algorithm in the add-on processor can determine if the PRI or TFI has changed. If changes are identified, the add-on system can update the new PRI and TFI values in 220.

**[0046]** At step 222, the add-on processor proceeds again to step 216 and continues to collect new data. The add-on processor continues to evaluate data at step 218 and updates the PRI and TFI if changes are identified.

**[0047]** Figs. 3A-3B illustrate another embodiment of an external add-on system 300 for use with a host ultrasound system 302 and host transmit/receive probe 304 to image tissue 301, the system further including high impedance taps 314 to connect the add-on system to the host system and probe. The taps 314 can be wires, for

example. In Figs. 3A-3B, host ultrasound system 302, host transmit/receive probe 304, receiving probes 306 and 308, add-on processor 310, and display 312 can correspond, respectively, to host ultrasound system 102, host transmit/receive probe 104, receiving probes 106 and 108, add-on processor 110, and display 112 of Figs. 1A-1B. The taps 314 can connect from host probe 304 to add-on processor 310 to detect the start time and direction of the pulses transmitted from the host probe. In

5 this configuration, all of the transmit pulses can be available to the add-on processor via the taps, instead of needing an algorithm to synchronize the add-on system to the host system as described above with reference to Figs. 1A-1B and Fig. 2.

**[0048]** The taps 314 can wire into the transmit/receive probe of the host machine in order to detect directly the start of the transmit pulse. Also, by using this method, the direction of each transmitted pulse can be determined by monitoring the start pulse on a subset of two or more

10 elements of the transmit array. In most current sector scan machines, the direction of the transmit beams progresses monotonically from one side of the sector to the other. In some advanced host machines, the beams may not be sent out in equal increments of angle from one pulse to the next, but instead may be transmitted in some interlaced order. When working with such a machine, it would be necessary to calculate the direction of each transmit pulse.

**[0049]** Another embodiment of a method of synchronizing an add-on ultrasound system to a host ultrasound probe will now be described. Referring to add-on system 300 of Figs. 3A-3B, host ultrasound probe 304 can transmit ultrasound pulses into tissue 301. The transmitted pulses can be received by the add-on system, such as

20 by receiving probe 306. In some embodiments, such as in Fig. 3B, the add-on system can include a plurality of receiving probes for receiving the transmitted ultrasound signals (e.g., receiving probes 306 and 308). Add-on processor 310 can then synchronize the add-on system to the host ultrasound probe using data from tap 314 that couples the host ultrasound probe to the add-on system. When the add-on system is synchronized to the host ultrasound probe, the add-on system can provide high-resolution images of the target tissue being imaged to a display, such as to a GUI.

**[0050]** As for additional details pertinent to the present invention, materials and manufacturing techniques may be employed as within the level of those with skill in the relevant art. Reference to a singular item, includes the 25 possibility that there are plural of the same items present. More specifically, as used herein and in the appended claims, the singular forms "a," "and," "said," and "the" include plural referents unless the context clearly dictates otherwise. Unless defined otherwise herein, all technical and scientific terms used herein have the same meaning as commonly understood by one of ordinary skill in the art to which this invention belongs.

**Claims**

1. A method of synchronizing an add-on ultrasound system (100, 300) to a host ultrasound probe (102, 104, 302, 304) for producing ultrasound images using multiple apertures, comprising:

transmitting ultrasound pulses from the host ultrasound probe;

receiving the ultrasound pulses with the add-on ultrasound system; and

synchronizing the add-on ultrasound system to the host ultrasound probe with an algorithm in a processor (110, 310) that calculates a start of frame of the transmitted ultrasound pulses by one of the following:

(i) identifying an interval between amplitude peaks that is substantially larger than a pulse repetition interval;

(ii) identifying a large change in peak amplitudes during successive scan lines; or

(iii) identifying when a peak amplitude changes from a low to a high or vice versa.

2. The method of claim 1, wherein the receiving step further comprises receiving the ultrasound pulses with a receiving probe (106, 306) or with a plurality of receiving probes (106, 108, 306, 308) of the add-on ultrasound system (100, 300).

3. The method of any claim 1 or 2, wherein the synchronizing step further comprises synchronizing the add-on ultrasound system (300) to the host ultrasound probe (302, 304) with the processor (310) adapted to process data from a tap (314) that couples the host ultrasound probe to the add-on system.

4. The method of any one of the preceding claims further comprising providing ultrasound images to a display (112, 312) from the add-on ultrasound system (100, 300).

5. An add-on ultrasound system (100, 300), comprising:

an ultrasound receiver (106, 306) configured to receive ultrasound pulses transmitted from a host probe (102, 104, 302, 304);

a processor (110, 310) coupled to the ultrasound receiver, the processor comprising an algorithm configured to synchronize the add-on system to the host probe for producing ultrasound images using multiple apertures, wherein the algorithm is adapted to calculate a start of frame of the transmitted ultrasound pulses by one of the following:

(i) identifying an interval between amplitude peaks that is substantially larger than a pulse repetition interval;

(ii) identifying a large change in peak amplitudes during successive scan lines; or

(iii) identifying when a peak amplitude changes from a low to a high or vice versa.

6. The add-on ultrasound system of claim 5 further comprising a display (112, 312) adapted to display ultrasound images from the processor (110, 310).

7. The add-on ultrasound system of claim 5 or 6 further comprising a second ultrasound receiver (108, 308).

8. The add-on ultrasound system of any one of claims 5 to 7 further comprising a tap (314) coupling the host ultrasound probe (302, 304) to the add-on system (300).

9. The add-on ultrasound system of claim 8, wherein the processor (310) is adapted to process data from the tap (314) to synchronize the add-on system (300) to the host ultrasound probe (302, 304).

**Patentansprüche**

1. Verfahren zum Synchronisieren eines Add-on-Ultraschallsystems (100, 300) mit einer Host-Ultraschallsonde (102, 104, 302, 304) zum Erzeugen von Ultraschallbildern unter Verwendung von mehreren Aperturen, das Folgendes umfasst:

Übertragen von Ultraschallimpulsen von der Host-Ultraschallsonde;

Empfangen der Ultraschallimpulse mit dem Add-on-Ultraschallsystem; und

Synchronisieren des Add-on-Ultraschallsystems mit der Host-Ultraschallsonde mit einem Algorithmus in einem Prozessor (110, 310), der einen Start eines Rahmens der übertragenen Ultraschallimpulse durch eines der Folgenden berechnet:

(i) Identifizieren eines Intervalls zwischen Amplitudenhöchstwerten, das wesentlich größer ist als ein Impulswiederholungintervall;

(ii) Identifizieren einer großen Änderung von Höchstwertamplituden während aufeinanderfolgenden Scanlinien; oder

(iii) Identifizieren, wann sich eine Höchstamplitude von einem Tiefpunkt zu einem Höchstpunkt oder umgekehrt ändert.

2. Verfahren nach Anspruch 1, wobei der Empfangsschritt ferner Empfangen der Ultraschallimpulse mit

einer Empfangssonde (106, 306) oder mit einer Vielzahl von Empfangssonden (106, 108, 306, 308) des Add-on-Ultraschallsystems (100, 300) umfasst.

3. Verfahren nach einem der Ansprüche 1 oder 2, wobei der Synchronisationsschritt ferner das Synchronisieren des Add-on-Ultraschallsystems (300) mit der Host-Ultraschallsonde (302, 304) mit dem Prozessor (310) umfasst, der dazu ausgelegt ist, Daten aus einer Leitung (314) zu verarbeiten, welche die Host-Ultraschallsonde an das Add-on-System koppelt.

4. Verfahren nach einem der vorhergehenden Ansprüche, das ferner Bereitstellen von Ultraschallbildern an einer Anzeige (112, 312) von dem Add-on-Ultraschallsystem (100, 300) umfasst.

5. Add-on-Ultraschallsystem (100, 300), das Folgendes umfasst:

einen Ultraschallempfänger (106, 306), der dazu konfiguriert ist, Ultraschallimpulse zu empfangen, die von einer Host-Sonde (102, 104, 302, 304) übertragen werden;

einen Prozessor (110, 310), der an den Ultraschallempfänger gekoppelt ist, wobei der Prozessor einen Algorithmus umfasst, der dazu konfiguriert ist, das Add-on-System mit der Host-Sonde zum Erzeugen von Ultraschallbildern unter Verwendung mehrerer Aperturen zu synchronisieren, wobei der Algorithmus dazu ausgelegt ist, einen Start eines Rahmens der übertragenen Ultraschallimpulse durch eines der Folgenden zu berechnen:

(i) Identifizieren eines Intervalls zwischen Amplitudenhöchstwerten, das wesentlich größer ist als ein Impulswiederholungsintervall;

(ii) Identifizieren einer großen Änderung von Höchstwertamplituden während aufeinanderfolgenden Scanlinien; oder

(iii) Identifizieren, wann eine Höchstwertamplitude von einem Tiefpunkt zu einem Höchstpunkt oder umgekehrt wechselt.

6. Add-on-Ultraschallsystem nach Anspruch 5, das ferner eine Anzeige (112, 312) umfasst, die dazu ausgelegt ist, Ultraschallbilder von dem Prozessor (110, 310) anzuzeigen.

7. Add-on-Ultraschallsystem nach Anspruch 5 oder 6, das ferner einen zweiten Ultraschallempfänger (108, 308) umfasst.

8. Add-on-Ultraschallsystem nach einem der Ansprü-

che 5 bis 7, das ferner eine Leitung (314) umfasst, welche die Host-Ultraschallsonde (302, 304) an das Add-on-System (300) koppelt.

5 9. Add-on-Ultraschallsystem nach Anspruch 8, wobei der Prozessor (310) dazu ausgelegt ist, Daten aus der Leitung (314) zu verarbeiten, um das Add-on-System (300) mit der Host-Ultraschallsonde (302, 304) zu synchronisieren.

## Revendications

1. Procédé de synchronisation d'un système ultrasono à ajouts (100, 300) à une sonde ultrasonore hôte (102, 104, 302, 304) pour produire des images ultrasonores grâce à de multiples ouvertures, comprenant :

l'émission d'impulsions ultrasonores à partir de la sonde ultrasonore hôte ;

la réception des impulsions ultrasonores avec le système ultrasonore à ajouts ; et

la synchronisation du système ultrasonore à ajouts à la sonde ultrasonore hôte avec un algorithme dans un processeur (110, 310) qui calcule un début de trame des impulsions ultrasonores émises par l'un des moyens suivants :

(i) identification d'un intervalle entre les pics d'amplitude qui est sensiblement plus grand qu'un intervalle de répétition d'impulsion ;  
 (ii) identification d'une grande variation dans les amplitudes de pic lors de lignes successives de balayage ; ou  
 (iii) identification du moment où une amplitude de pic passe d'un point bas à un point haut ou vice versa.

40 2. Procédé selon la revendication 1, dans lequel l'étape de réception comprend en outre la réception des impulsions ultrasonores à l'aide d'une sonde réceptrice (106, 306) ou d'une pluralité de sondes réceptrices (106, 108, 306, 308) du système ultrasonore à ajouts (100, 300).

3. Procédé selon l'une quelconque des revendications 1 ou 2, dans lequel l'étape de synchronisation comprend en outre la synchronisation du système ultrasonore à ajouts (300) avec la sonde ultrasonore hôte (302, 304) par le processeur (310) conçu pour traiter les données à partir d'un robinet (314) qui couple la sonde ultrasonore au système d'ajouts.

55 4. Procédé selon l'une quelconque des revendications précédentes, comprenant en outre l'utilisation d'images ultrasonores sur un dispositif d'affichage (112, 312) à partir du système ultrasonore à ajouts (100,

300).

5. Système ultrasonore à ajouts (100, 300) comprenant :

5

un récepteur ultrasonore (106, 306) configuré pour recevoir des impulsions ultrasonores émises à partir d'une sonde hôte (102, 104, 302, 304) ;  
 un processeur (110, 310) couplé au récepteur ultrasonore, le processeur comprenant un algorithme configuré pour synchroniser le système d'ajouts à la sonde hôte pour produire des images ultrasonores grâce à de multiples ouvertures, l'algorithme étant adapté pour calculer un début de trame des impulsions ultrasonores émises par l'un des moyens suivants :

(i) identification d'un intervalle entre les pics d'amplitude qui sont sensiblement plus grands qu'un intervalle de répétition d'impulsion ;  
 (ii) identification d'une grande variation des amplitudes de pic lors de lignes successives de balayage ; ou  
 (iii) identification du passage d'une amplitude de pic d'un point bas à un point haut ou vice versa.

6. Système ultrasonore à ajouts selon la revendication 5, comprenant en outre un dispositif d'affichage (112, 312) conçu pour afficher des images ultrasonores à partir du processeur (110, 310).

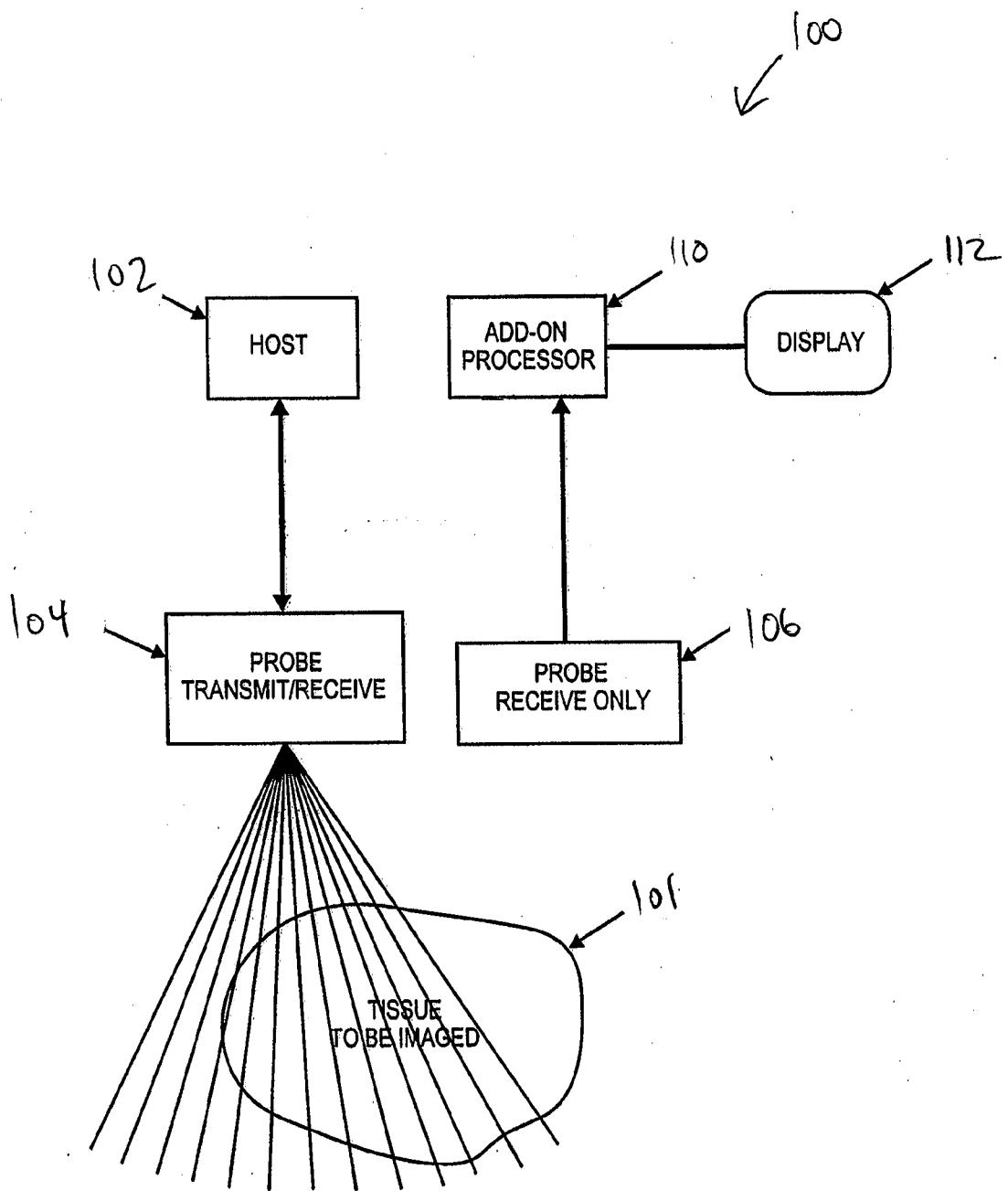
7. Système ultrasonore à ajouts selon la revendication 5 ou 6, comprenant en outre un récepteur ultrasonore (108, 308).

8. Système ultrasonore à ajouts selon l'une quelconque des revendications 5 à 7, comprenant en outre un robinet (314) couplant la sonde ultrasonore hôte (302, 304) au système à ajouts (300).

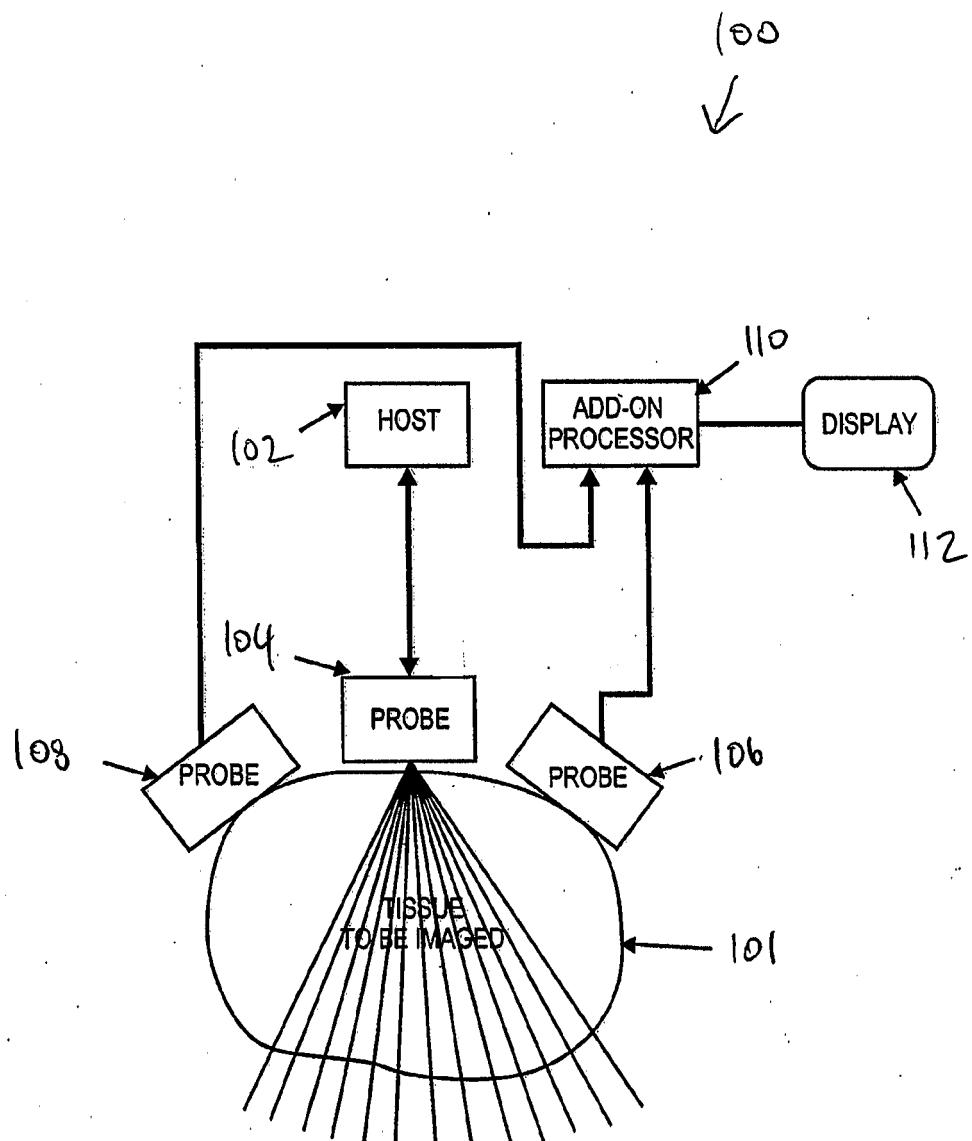
9. Système ultrasonore à ajouts selon la revendication 8, dans lequel le processeur (310) est adapté pour traiter des données provenant du robinet (314) pour synchroniser le système à ajouts (300) à la sonde ultrasonore hôte (302, 304).

50

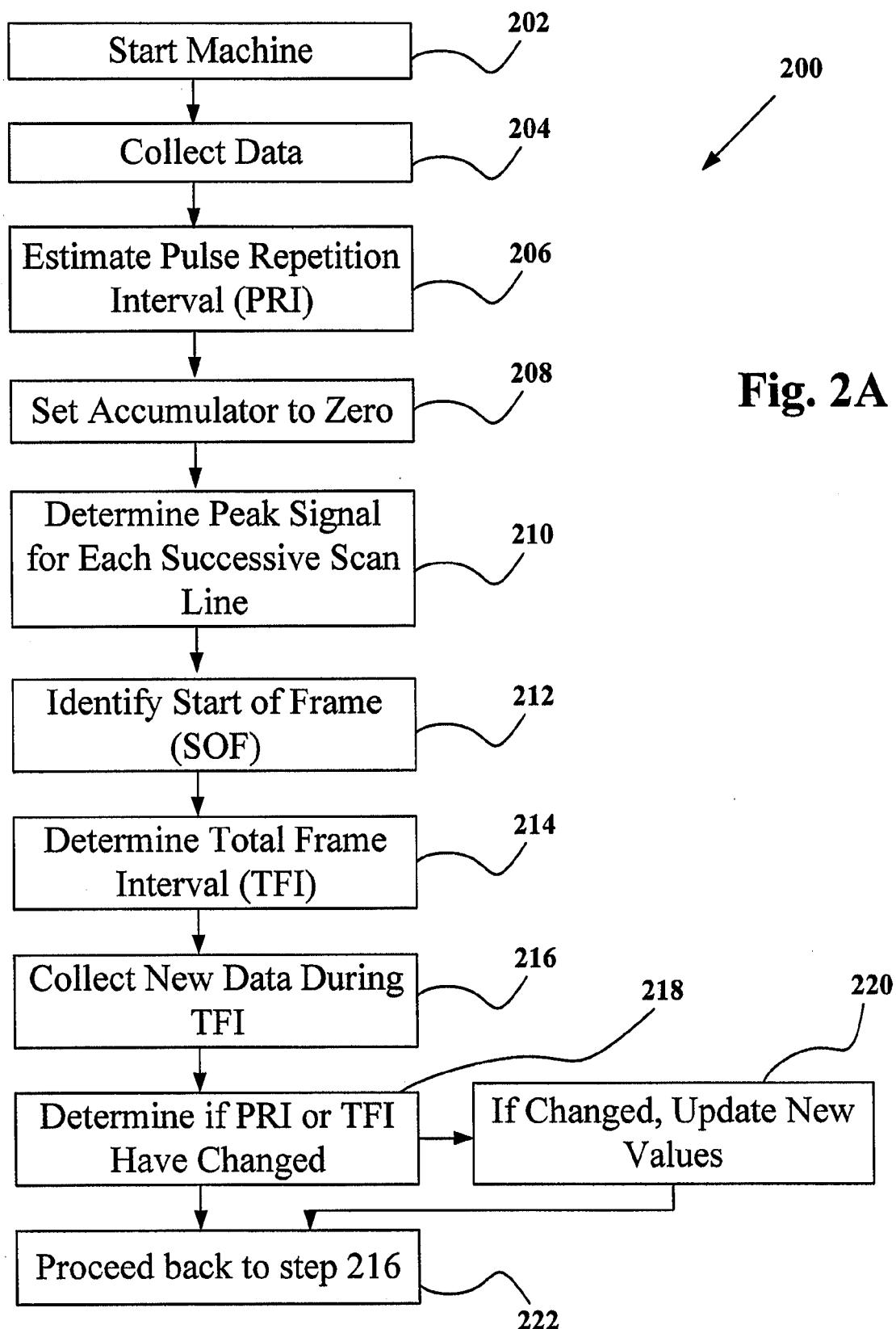
55



**FIG. 1A**



**FIG. (B)**

**Fig. 2A**

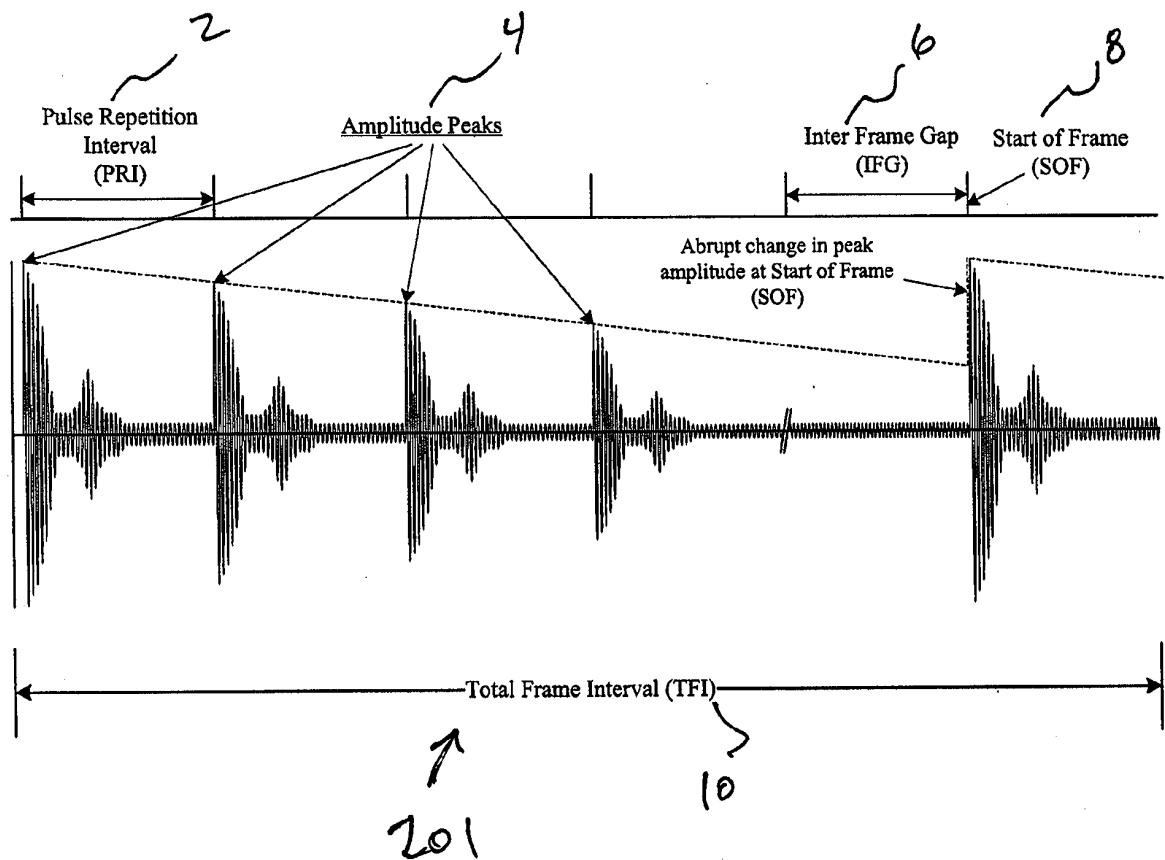
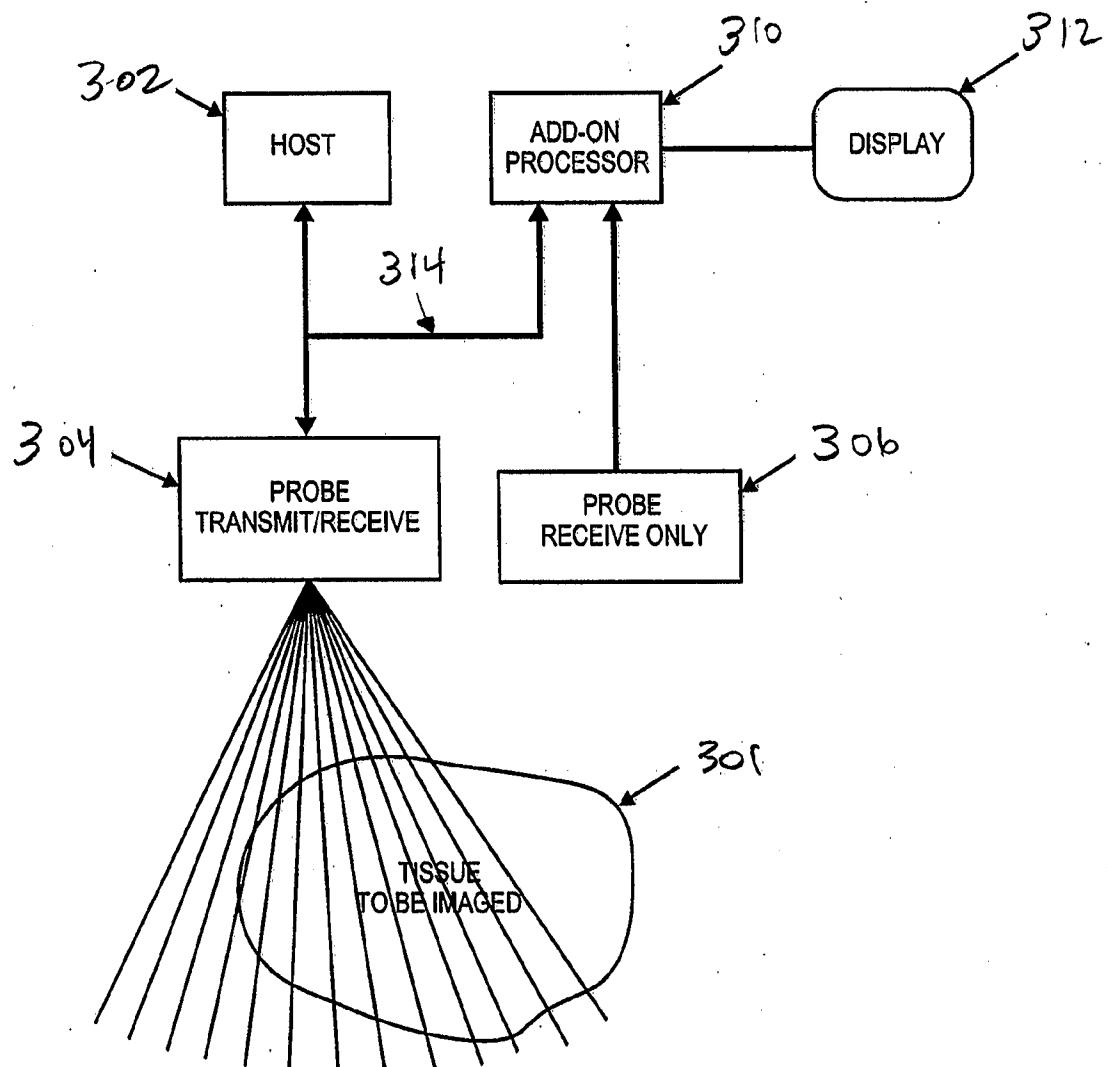
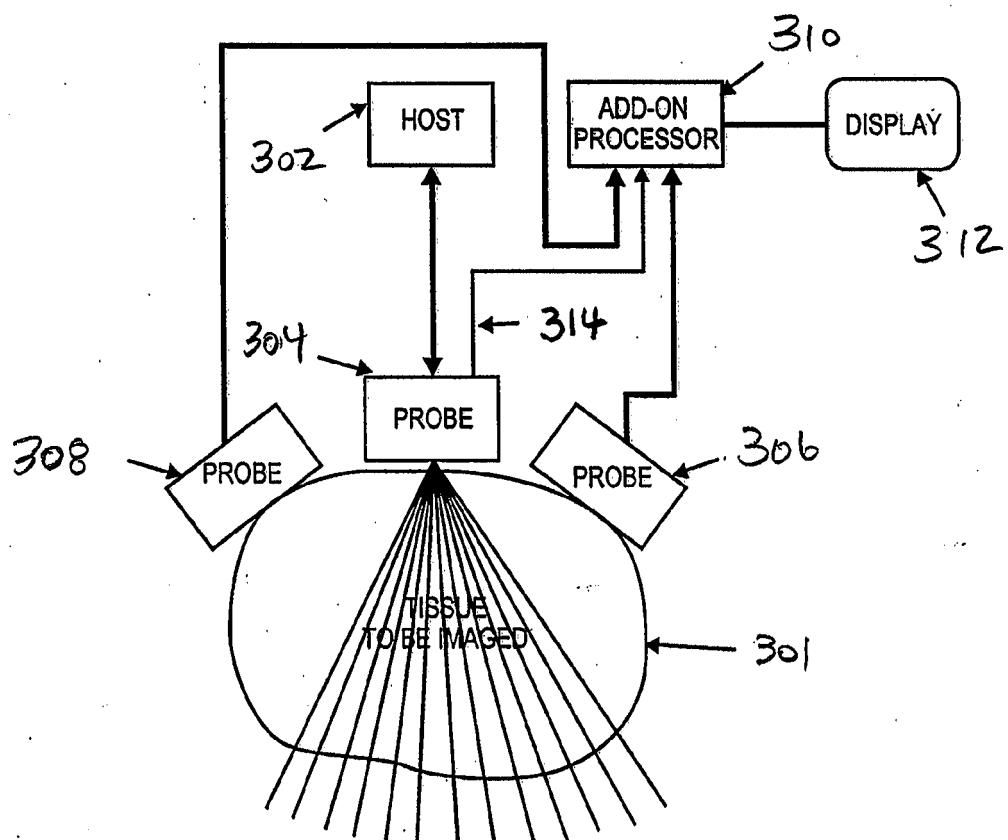


FIG. 2B



**FIG. 3A**



**FIG. 3B**

**REFERENCES CITED IN THE DESCRIPTION**

*This list of references cited by the applicant is for the reader's convenience only. It does not form part of the European patent document. Even though great care has been taken in compiling the references, errors or omissions cannot be excluded and the EPO disclaims all liability in this regard.*

**Patent documents cited in the description**

- US 5355888 A [0008]
- US 20060270934 A [0009]

**Non-patent literature cited in the description**

- **HARVEY FEIGENBAUM.** Echocardiography. Lippincott Williams & Wilkins, 1993 [0003]
- **P. N. T. WELLS.** Biomedical Ultrasonics. Academic Press, 1977 [0004]

专利名称(译)	使用多孔径医疗超声成像和附加系统同步		
公开(公告)号	<a href="#">EP2320802B1</a>	公开(公告)日	2018-08-01
申请号	EP2009805593	申请日	2009-08-07
[标]申请(专利权)人(译)	茂伊成像股份有限公司		
申请(专利权)人(译)	MAUI IMAGING , INC.		
当前申请(专利权)人(译)	MAUI IMAGING , INC.		
[标]发明人	SPECHT DONALD F BREWER KENNETH D		
发明人	SPECHT, DONALD, F. BREWER, KENNETH, D.		
IPC分类号	A61B8/00 G01N29/24 G01N29/36 G01S15/89 G01S7/52		
CPC分类号	A61B8/4477 A61B8/54 G01S7/52046 G01S7/52087 G01S15/8913 G01S15/8927 G01S15/8929 G01S15/8997 A61B8/00 A61B8/4281 A61B8/5207		
代理机构(译)	POTTER CLARKSON LLP		
优先权	61/087571 2008-08-08 US 61/169264 2009-04-14 US		
其他公开文献	EP2320802A2 EP2320802A4		
外部链接	<a href="#">Espacenet</a>		

#### 摘要(译)

使用附加设备可以实现多孔径超声探头的优势。来自位于不同阵列中的多个换能器元件的回波的同步和相关对于多孔径成像的成功处理是必不可少的。这里公开的算法教导了当传输源来自另一个超声系统并使附加系统与另一个超声系统同步时成功处理这些信号的方法。具有不同噪声分量的二维图像可以由各个换能器元件接收的回波构成。所公开的技术在医学成像中具有广泛的应用，并且理想地适合于使用两个或更多个肋间空间的多孔径心脏成像。

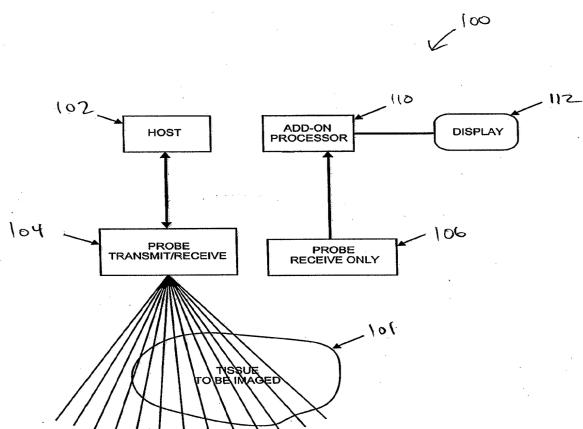


FIG. 1A