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(54) EXTENDED FIELD OF VIEW ULTRASONIC DIAGNOSTIC IMAGING WITH IMAGE REACQUISITION

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IMAGERIE DIAGNOSTIQUE ACOUSTIQUE A CHAMP DE VISON ETENDU AVEC REACQUISITION D'IMAGES

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- "Y. Hara et al.: "A New Sonographic Technique for Assessing Carotid Artery Disease: Extended- Filed-of-View Imaging"; American Journal of Neuroradiology, Vol. 20, February 1999; pages 267-270"

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Description

[0001] This invention relates to ultrasonic diagnostic imaging systems and, in particular, to ultrasonic diagnostic imaging systems which produce ultrasonic images with an extended field of view.

5 [0002] Ultrasonic diagnostic imaging systems of the 1970s and 1980s were manufactured with what is known as B-arm scanning. In B-arm scanning systems an A line (single beam) transducer was mounted at the end of an articulated arm. The joints of the articulated arm contained sensors which continuously monitored the relative positions of the arm segments, enabling the spatial position of the transducer to be constantly tracked. As the transducer was scanned over the body of the patient, the relative spatial locations of consecutive A lines was computed from the articulated arm 10 sensors, and the A lines were assembled in consecutive, side-by-side locations on an image display. The B arm system was thus capable of painting an ultrasonic image that could laterally extend for the maximum number of successive A lines that the system could store and display and over which the B arm could extend.

15 [0003] In recent years electronically scanned array transducers have been adapted for the same purpose. Since an electronically scanned array transducer automatically produces a two dimensional image, movement of the array transducer in the plane of the image will produce successive, spatially offset two dimensional images. Each new image in a new spatial location can be spatially registered with a previously acquired image with which it overlaps, then combined with the previous images to produce an extended image which is laterally extensive in the direction of motion of the array transducer. The extent of the extended field of view image is determined by the capacity of the ultrasound system to store and display multiple partially overlapping two dimensional images.

20 The article entitled "A New Sonographic Technique for Assessing Carotid Artery Disease: Extended-Field-of-View Imaging" by Y. Hara et al, published in the American Journal of Neuroradiology, Vol. 20, February 1999, pages 267-270, describes an extended field of view (EFOV) imaging technique. An operator moves a transducer slowly in a lateral direction over a region of interest. A global transformation (translocation and rotation) is calculated from local motion vectors to describe the motion of the transducer from frame (k-1) to frame (k). Using the global motion information from 25 each frame, software smoothly blends the individual frames in a successive manner to generate a composite panoramic image. The algorithm allows the operator to halt during forward transducer movement or to move backward to correct part of the acquired composite image.

30 Extended field of view (EFOV) imaging systems of the prior art are capable of producing a continuous EFOV image as a scanhead is continually moved in a given direction along the surface of the body. However, a clinician acquiring an EFOV image is often trying to image a structure of extended length in the body, such as a blood vessel in an arm or leg. Although the clinician is trying to maintain the vessel in alignment with the image plane of the scanhead, frequently the path of the vessel and the moving scanhead will move out of alignment and the vessel will no longer appear in the image. In such circumstances, the usual recourse is to repeat the scan from the beginning. It would be desirable for the clinician 35 to compensate for the premature termination of the scan by being able to reacquire the blood vessel in the EFOV image.

35 To this effect, the present invention is a method of operating an ultrasonic diagnostic imaging system according to claim 1 and an ultrasonic imaging system according to claim 3. If the scanhead moves such that structure of interest is out of the scan plane of the EFOV image, the clinician may reverse the direction of the scan until the structure is reacquired, preferably at the point at which it initially disappeared from view. The clinician can therefore recover from misalignment 40 of the structure of interest and the scan plane and continue the scan without having to restart the scan from the beginning.

[0004] In the drawings:

45 FIGURE 1 illustrates the technique for scanning an array transducer to produce an extended field of view image; FIGURE 2 illustrates an extended field of view ultrasonic diagnostic imaging system constructed in accordance with the principles of the present invention;

FIGURES 3a-3d illustrate image registration using a set of images exhibiting different levels of resolution;

FIGURES 4a-4c illustrate SAD characteristics for images of different levels of resolution;

FIGURES 5a and 5b illustrate three overlapping elemental images which form an extended field of view image;

FIGURE 6 depicts the organization of an extended field of view history buffer;

FIGURES 7a-7c illustrate how successive elemental images are entered into the history buffer of FIGURE 6;

50 FIGURES 8a-8b illustrate the assembly of an extended field of view ultrasonic image from the central portions of successive elemental ultrasonic images; and FIGURES 9a-9e illustrate the reacquisition of a blood vessel in an EFOV image by reversal of the scanning direction.

55 [0005] Referring first to FIGURE 1, the technique for scanning an array transducer to produce an extended field of view image is shown. An ultrasonic scanhead 10 which includes an electronically scanned array transducer 12 is shown in contact with the skinline 94 of a patient. In this example the clinician wants to scan a length of blood vessels 90,92,94, and to display the blood vessels in an extended field of view image. As the drawing shows, only the narrow region of the bifurcation 96 is directly beneath the aperture of the array transducer 12 and hence viewable in a single conventional

image. To scan a length of the blood vessels, the clinician slides the scanhead in the direction 14, which denotes a direction co-aligned with the longitudinal axis of the array transducer and the plane of an image. As the scanhead is moved in the direction 14, successive planar images referred to herein as elemental images are acquired, each being slightly displaced (as a function of the speed of scanhead motion and the image acquisition rate) in the direction 14 from the previous image. The displacement between successive elemental images is computed and the images are registered and combined on the basis of the displacements to produce a composite extended field of view image of the blood vessels.

[0006] Ideally, it is desirable for the scanhead to be translated at a constant speed while images are acquired, so that individual elemental images are not stretched or compressed laterally relative to earlier acquired elemental images. It is also desirable for the scanhead to be moved in a single plane, so that there is high correlation from each elemental image to the next. However, manual scanning over an irregular body surface often causes departures from either or both of these desirable conditions. As will be seen below, the present invention provides solutions to the effects of less than desirable manual scanning.

[0007] An ultrasonic diagnostic imaging system for producing extended field of view images in accordance with the principles of the present invention is shown in FIGURE 2.

The scanhead 10 is moving in the direction 14 of the planes of successively acquired images F_{n-4} - F_n . The acquired images F_{n-4} - F_n are transparently shown in this drawing so that their spatial overlap can be appreciated. The first image acquired in this sequence is image frame F_{n-4} , and the last image acquired is frame F_n , shown in alignment with the aperture of the array transducer 12. The echoes of each acquired image frame are formed into beams by beamformer 20. The coherent echoes are then processed by a signal processor 22 and arranged in respective ultrasonic images by a scan converter 24. To form conventional real time images, each image is coupled to a video processor 26 and displayed on an image display 30.

[0008] In accordance with the principles of the present invention, each image is coupled to an EFOV image processor 40. The EFOV image processor, which may operate with either estimate data (pre-scan converted) images or display data (scan converted pixel data) images, receives each newly acquired image during the EFOV mode of operation and computes the displacement between the new image and the previously acquired elemental image of the EFOV image, as more fully described below. The EFOV image processor stores the new image in registration with the previously acquired elemental images in an extended image memory 42 as described below. Each time the EFOV image is extended by the addition of new image data, the EFOV image data stored in the extended image memory 42 is extracted from the memory and combined by a combiner 44 to form a new EFOV image, which is coupled to the video processor 26 for viewing on the display.

[0009] FIGURES 3a-3d illustrate a preferred technique in accordance with the present invention for computing the displacement between images so that multiple offset elemental images may be registered and combined into a single EFOV image. The two images which are to be registered can be the newly acquired elemental image and the previously formed EFOV image. In the preferred embodiment of the present invention the newly acquired elemental image is registered with the previously acquired elemental image. The first step is to process each image into a set of images of different levels of resolution. The starting images have the highest resolution in the set, and each additional image in the set exhibits progressively coarser resolution. A set of four such images is shown in FIGURES 3a-3d, with image 32 being the received elemental image, and each of the other images 34, 36, and 38 having progressively coarser resolution. Images 34, 36, and 38 can be produced by a variety of methods. Images 34, 36 and 38 can be produced by passing image 32 through low pass filters of progressively lower cutoff frequencies. Images 34, 36 and 38 can be produced by successive downsampling and/or truncating of the image data of image 32. As FIGURES 3a-3d show, each image of progressively coarser resolution clearly shows only image features of increasing significance in the image. For instance, the highly resolved mitten-shaped structure 50 in image 32 shows less fine detail in the same structure 52 in the lower resolution image 34 of FIGURE 3b. Only higher level details of the same structure 54 are seen in the lower resolution image 36 of FIGURE 3c, and only the highest level outline 56 of the same structure is seen in the lowest level resolution image 38 of FIGURE 3d. One way to segment the levels of resolution is to produce an image 34 with half the resolution of the original image 32, an image 36 with half the resolution of image 34, and an image 38 with half the resolution of image 36.

[0010] In the next step in the process, the lowest resolution image 38 from two elemental images are compared with each other to ascertain the spatial displacement between the two. In a preferred embodiment, only a small area around a single point in the image is used for the comparison. The point can be the location of a prominent feature in the image or an arbitrary point such as the center of the image. A suitable area over which to perform the comparison is an eight pixel by eight pixel area 60 around the point indicated by the "+" symbol in FIGURE 3d. The areas 60 of the two images are aligned in various ways to determine the alignment in which the coarsely defined feature(s) in the area are most closely in congruence. A systematic way for performing these alignments is to carry out a sum absolute difference (SAD) search of the pixels around the + point in each image to determine the minimum SAD which indicates the best match. The SAD search compares pixels P by performing comparisons in accordance with the algorithm

$$\sum_{y=0}^8 \sum_{x=0}^8 |P_{n(x-x-dx, y-y-dy)} - P_{o(x-x, y-y)}|$$

5 Where P_n is a pixel of the newly acquired image, P_o is a pixel of a previous (old) image, x and y are the parameters over which the summations are performed, and X and Y are the reference coordinates of the feature in the pixel area, generally at the center of the area. The algorithm is iterated for alignment offsets dx,dy until min SAD(X,Y,dx,dy) is found. As the SAD search is being carried out, boundary conditions are constantly checked to ascertain whether a result is a true minimum or only an aberrational value. For example, a minimum SAD occurring when the center point + of one area is aligned with the edge of the search area would be ignored. Minimum SAD values are also compared against thresholds for validity in terms of both magnitude and percentage values. Each SAD calculation includes a comparison against the condition of no offset, where the displacement parameters are set to zero. Since the images being compared are of the coarsest resolution level, only the most significant features of the image will be present in the data sets, and the process will result in the closest alignment of these significant image features.

10 [0011] Once a min SAD value has been found for the two pixel areas the parameter estimate is refined by a gradient search algorithm. This algorithm computes the differentials of the SAD value as a function of small offsets in each of the displacement parameter dimensions (x,y,θ) used to compute the min SAD. If an offset results in an improved SAD value, the displacement parameters are replaced with the refined offset parameters. The refinement process can be iteratively 15 repeated a number of times, each with an increasingly finer offset.

20 [0012] In the next step, the same comparison is made of the old and new images of the next highest level of resolution. This time, the comparison is made using a greater number of small image areas such as those indicated by the small 25 boxes 60,62 in FIGURE 3c. The points + around which the areas are located can be chosen arbitrarily but preferably are chosen to include identified image features. In FIGURE 3c the location of box 60 is arbitrarily chosen, while box 62 is defined to be located on features of image structure 54. Again a systematic comparison of corresponding pixel areas such as a min SAD search is performed. Preferably, the alignment analysis for the second and subsequent resolution 30 levels begins with the two images initially aligned (pre-warped) as determined by the displacement measure resulting from the analysis of the previous level. Before applying the displacement parameters of the previous level it may be necessary to scale them, as there may be differences in pixel size and/or density from one level to the next due to the resolution difference.

35 [0013] At the second and subsequent resolution levels where multiple small pixel areas 60,62 are analyzed for min SAD, a predetermined number of the areas must yield a valid min SAD value before the previous displacement parameter values will be replaced by new ones. For example, if the comparisons of at least three of the four areas 60,62 of the second resolution level each yield a valid minimum SAD, then the three or four results are aggregated and used as the 40 new displacement parameters. If less than three areas yield a valid min SAD, then the results are discarded and the parameters of the image comparison at the previous resolution level are retained as the preferred displacement parameters. Again, boundary conditions are checked to prevent aberrational results from being used as registration parameter values.

45 [0014] Two more registration analyses of the two higher resolution image sets 34 and 32 are performed in accordance with this same process. Preferably, the analyses at the higher resolution levels are performed with a greater number of pixel areas of comparison. For example up to sixteen areas 60,62 can be used in the comparisons involving images 34 and 32, with each pixel area preferably chosen to correspond with a significant feature in the image. Features are defined as regions of the image that contain structures that can be matched accurately and robustly such as points and corners. If the results of these comparisons yield better parameter values, the new displacement parameters are used. If no 50 better parameters are found, the previous results are retained as the displacement parameters. The gradient refinement process can be applied at these higher resolution levels by using a number of feature areas or arbitrarily chosen points at different image locations, retaining displacement parameters which yield an improved overall min SAD result. These refined parameters are then used to align the new elemental image with the previous elemental image of the EFOV image. The new elemental image is added to the previous images in a history buffer as described below in conjunction with FIGURES 5-7.

55 [0015] Prior art techniques for measuring image displacement are generally computationally intensive. That shown in U.S. Pat. 5,566,674, for instance, performs a computation for every pixel area of each entire high resolution image. The technique of the present invention does not require such intensive processing, relying as it does on comparisons of just a few small, discrete areas of each image. Improved accuracy and robustness are provided by the use of multi-resolution levels of the same image which tend to produce fewer local minima, and the use of feature-based comparisons, rather than blindly processing all the data of every image. This is illustrated by the SAD characteristics of FIGURES 4a-4c.

[0016] The use of multiple small pixel areas for alignment analysis permits accurate alignment of elastically deformed images. For example, an elemental image may be laterally stretched or compressed relative to the previous elemental

image by reason of changes in the speed at which the scanhead is moved during scanning. Image deformation within an image can occur due to motion of the anatomy being scanned, such as the heart. If scanhead motion is increasing, a new image can be stretched in relation to a previous image, and can be relatively compressed if scanhead motion is decreasing. The degree of elasticity is a function of both scanhead motion and the directional sequence in which the scanlines of the image are transmitted. By computing min SAD at a plurality of separate image areas 60,62, separate portions of the old and new images can be separately aligned. Registration parameters for intermediate image regions can be scaled in proportion to the parameters calculated for the specific areas 60,62. Thus, elastic deformation errors can be overcome and eliminated from the registration process.

[0017] FIGURE 4a illustrates a typical SAD characteristic 100 for a full resolution image 32 which might result from the calculation and plotting of a complete SAD characteristic for an alignment parameter. In a constructed embodiment of the present invention only a few points of such a SAD characteristic are computed and compared as the processor 40 tries to locate the minimum SAD point 108. Due to the high spatial frequency content of the high resolution image 32, the SAD characteristic is likely to exhibit points 104,106 of local minima in addition to the overall minimum 108. This can be due to alignment of image artifacts such as speckle, for instance. Thus, the SAD analysis can lead to identification of a point 102 that is approaching a local minimum 104, rather than the overall characteristic minimum 108.

[0018] However, the use of different image resolution levels will cause the SAD characteristics of the coarser resolution level images to exhibit far less high spatial frequency content. Accordingly, the SAD characteristics of these lower resolution renditions will appear as shown by SAD characteristic 110 of FIGURE 4b, in which the local minima of the high resolution SAD characteristic are smoothed over. Thus, an initial estimate of the minimum SAD point may be located at point 112 and approaching the overall characteristic minimum 108 rather than some local minima. The initial pre-warping, gradient refinement processing, and iterative SAD computations at higher levels of resolution will cause an initial min SAD estimate 114 to iteratively progress to points 116 and 118, as shown in FIGURE 4c, to progressively home in on the desired minimum SAD point 108.

[0019] When the displacement necessary to align a new elemental image to the previous elemental image in an EFOV series is known, the new elemental image can be combined with the others to produce an extended image. One way to do this is to employ an EFOV image buffer 42 in which a single EFOV image formed from previously acquired elemental images is stored. The new elemental image is then added to the EFOV image in the buffer, generally through some form of weighting or averaging, to produce a new EFOV image for display. Once the new elemental image has been added to the EFOV image it can no longer be separately identified, as it is blended into and becomes an integral part of the EFOV image. In accordance with a further aspect of the present invention, it is preferable to use a history buffer for the image memory 42, in which the pixels of the individual elemental images continue to be separately distinguishable. FIGURE 6 depicts the organization of a preferred history buffer 130. The x,y coordinates of the history buffer 130 shown on the top surface 132 correspond to the maximum sight area of a displayed EFOV image. The column depth z of the history buffer is the maximum number of pixels of different elemental images which can be stored and combined to form each pixel of the EFOV image. In the illustrated embodiment the history buffer is shown to be six pixels deep as shown by delineations 132. In a constructed embodiment the history buffer may be eight to sixteen pixels deep.

[0020] Referring to FIGURE 5a, three exemplary elemental images A, B, and C are shown which are acquired as the initial elemental images for an EFOV image. Image A is the first to be acquired as the scanhead moves from left to right to acquire images A, B, and C in succession. Image A is therefore entered first into the history buffer 130 and is aligned to the left edge of the buffer as shown in FIGURE 6. If the scanhead were moving from right to left, the first image A would be aligned at the right side of the buffer so that the EFOV image could be extended from right to left instead of from left to right as depicted in this example. When the image A is entered into the history buffer, it completely fills the pixel storage areas (depth z) beneath its x,y coordinates with image A pixel values as shown in FIGURE 7a. FIGURES 7a-7c depict the history buffer cross-section in a plane 140 between arrows 7-7 in FIGURE 6. The remaining pixel storage areas of the history buffer continue to be set to invalid values at this time.

[0021] Image B is next acquired and aligned with image A as described above. Image B is stored in the history buffer in its aligned position in x,y coordinates with respect to image A. Where image B overlays image A, the image A pixels are "pushed down" by one pixel depth so that the upper pixel is occupied by pixel B and the remaining are still occupied by image A pixel values, as shown in FIGURE 7b. In areas where image B does not overlay image A, the full pixel depth is filled with image B pixel values.

[0022] When image C is acquired and aligned with image B the push down process is repeated as shown in FIGURE 7c. In the columns indicated by arrow 142 where all three images overlap, the top pixel is from image C, the next pixel down is from pixel B, and the remaining pixel depth is filled with image A pixels. In image areas where only images B and C overlap, the top pixel in the column is an image C pixel, and those below are image B pixels.

[0023] This process continues as additional elemental images are acquired to extend the EFOV image. The finite depth of the history buffer, six pixels in this example, limits the number of images which can overlap at any pixel location to the most recent six overlapping images. Older image pixels at the location are "pushed out" of the bottom of the buffer which, in the z direction, operates as a FIFO (first in, first out) buffer. This is unlike the above-described technique of

simply adding a new elemental image to an EFOV image, where an unlimited number of overlapping images are blended together. The finite limit of the history buffer provides a benefit of reduced image blurring as compared to the technique of simply recursively blending an EFOV image, since very old images in the history buffer overlay are removed by the FIFO push-down process. This is not possible where elemental images are blended into the EFOV image and are no longer separately distinguishable, unless each elemental image is stored and its position tracked for subsequent subtraction from the EFOV image. In addition the history buffer readily permits the scanning direction to be reversed during a scan. Another benefit is that the algorithm for combining elemental images into an EFOV image can be changed and different algorithms applied to the same extended image set.

[0024] Each time a new elemental image is added to the history buffer the combining algorithm is applied to the pixel data to form a pixel of an EFOV image from each column of pixels in the history buffer. It is seen that the initial filling of an entire column with pixels of the first image acquired at an x,y coordinate effects a weighting of the pixel data in favor of the initial image. If such weighting is not desired, the columns in the history buffer could only be filled one pixel depth at a time, or by another desired depth weighting. The combining algorithm may effect a summing of the pixel data at each column, an averaging or median filtering process, or some other linear or nonlinear filtering function (FIR, IIR, static, conditional, or adaptive) automatically or adaptively selected or chosen by the user. The EFOV image for elemental images A, B, and C would appear as shown by outline 120 in FIGURE 5b.

[0025] In accordance with a further aspect of the present invention, the full elemental image is not used in the EFOV image, but only the central portion of the elemental image, as shown in FIGURES 8a and 8b. FIGURE 8a shows an EFOV image 80 which is extended by a new elemental image 82. The full new elemental image 82 is that obtained by the full aperture of the array transducer, as delineated by bracket 70 above the new image 82. However, only the central portion of the new image 82, the portion that is above bracket 72 and comprises only approximately 20% of the full image width, is added to the EFOV image 80. This percentage can be adjusted depending upon scanning parameters such as the image acquisition or display frame rate. The central portion of the new image 82 is formed by the center of the array aperture, where the image is generally in its best focus. The central portion is formed by a balanced aperture, is (in the case of a phased array) steered directly ahead, and will most likely result from the best acoustic coupling to the body. Accordingly, since the central portion of the image is likely to be the most highly resolved image area, only the central area of the new elemental image is combined with the previously formed EFOV image. The resultant EFOV image with the addition of this central image area of elemental image 82 is illustrated in FIGURE 8b.

[0026] In addition to producing grayscale B mode images, most ultrasound systems produce images in which the motion or flow of tissue and fluids is depicted in color. Colorflow (velocity) imaging, Doppler power imaging, power motion imaging, and tissue Doppler imaging are modes in which motion and flow are imaged, either alone or in combination with B mode structural image data. In accordance with a further aspect of the present invention, two extended image memories 42 are used for EFOV images in these compound modes. Preferably two history buffers 130 are used, one in which the B mode image information is registered and stored, and a second in which the corresponding flow or motion image information is registered and stored. The use of two buffers allows flexibility in using different techniques for combining the elemental images of the two buffers into one EFOV image. In one approach, the combining algorithm first produces a B mode EFOV image from the data of one history buffer and a color EFOV image from the data of the other history buffer. These EFOV images can be alternately displayed or displayed simultaneously in different areas of the viewing screen. Alternatively, elemental images from the two buffers can be combined directly into an EFOV image based upon the distribution of the image data. For a composite EFOV image the combining algorithm combines the B mode and color data into a single EFOV image. The data of the two buffers is combined by preferentially using B mode data where data of both types is available at one EFOV pixel, by preferentially using color data when the color data exceed a predetermined threshold, or by blending the two together to form a pixel with a hue or color determined by characteristics of both data types.

[0027] In accordance with the principles of the present invention, a new elemental image is combined into an existing EFOV image irrespective of the direction 14 of scanhead motion. The process for measuring image displacement performs the analysis of image to image displacement for all directions, not just for the initial direction of scanhead motion. The EFOV image processor of FIGURE 2 will align and insert a new elemental image into the history buffer 130 regardless of the direction of the displacement needed to align the images. This means that the addition of a central area of a new elemental image may not extend the field of view of an EFOV image, but can instead overwrite completely within an existing elemental area of the EFOV image. This can, if desired, cause a decrease in the field of view rather than an increase. The use and benefit of this capability is illustrated in FIGURES 9a-9e.

[0028] FIGURES 9a-9e illustrate a procedure in which a clinician is trying to form an EFOV image 80 of the paths of blood vessels 92 and 94. The clinician is initially forming the EFOV image by moving the scanhead 10 in the direction of arrow 14a. But as FIGURE 9a illustrates, the clinician has unintentionally moved the scanhead such that the vessels 92 and 94 are no longer in the image plane of the transducer array 12. The portion of the EFOV image added by the most recently acquired elemental image, shown above bracket 72, does not follow the extension of vessels 92,94.

[0029] In accordance with the principles of the present invention, the clinician overcomes this difficulty by reversing

the direction of the scan, as shown by arrow 14b in FIGURE 9b. The portion of the EFOV image 80 of FIGURE 9b which has most recently been added is that shown above the bracket 72 at the center of the aperture of scanhead 10. As FIGURE 9b shows, this newly added image portion does not extend the EFOV image 80; instead it overwrites a portion of the EFOV image which is in the interior of the lateral dimensions of the image. The portion 82 of the previous EFOV

5 image to the right of the bracketed new area, shown outlined by dashed lines, is eliminated from the EFOV image. The EFOV image is now laterally reduced in size, as the reference to the former right side edge 84 of the EFOV image shows.

10 [0030] Functionally this process is defined by keeping track of the leading and trailing edges of the current elemental image. The leading edge of the image is the portion to the side of the central area (bracket 72) in which the scanhead is initially moved. The trailing edge of the image is the portion which follows the central area. The leading and trailing edges are defined initially when the scan direction is determined. When the registration parameters indicate that the direction of scanhead motion has changed, the processor 40 erases (invalidates) the pixel data in the history buffer which is in the leading edge region of each new elemental image added to the history buffer. In FIGURE 9b, as the scanhead moves to the left as shown by arrow 14b, the pixel data of the leading edge image area 84 which trails the central region (bracket 72) is erased and the entire column of each pixel of the history buffer filled in with invalid values, thereby eliminating that pixel data from the EFOV display.

15 [0031] The clinician continues to move the scanhead in the direction of arrow 14b until the blood vessels 92,94 are reacquired in the EFOV image plane, as shown in FIGURE 9c. The EFOV image 80 of FIGURE 9c contains a new elemental image area, that shown above the bracket 72 at the center of the scanhead aperture, in which an image of the blood vessels 92,92 has been reacquired in the plane of the rest of the EFOV image. The undesired out-of-plane EFOV image region at the leading edge (to the right) of the image portion above bracket 72, has been eliminated from the EFOV image, which has been shortened in width correspondingly. The new portion of the EFOV image above the bracket 72 shows structure not seen before, the bifurcation of one vessel 90 to form the two vessels 92,94. The new image portion is not obscured by old EFOV image data by reason of the finite depth of the history buffer 130, which has pushed the old unwanted image data down and out of the buffer.

20 [0032] With the blood vessels reacquired in the image, the clinician can resume scanning in the direction 14d, as shown in FIGURE 9d. The new elemental image portion of this EFOV image, shown above the bracket 72, reveals the extension of the blood vessels 92,94 as a single vessel 90. With continued motion in the direction of arrows 14d and 14e, the EFOV image 80 is fully filled in with the structure of blood vessels 90,92,94, as shown in FIGURE 9e. Thus it is seen that the clinician has the ability to overcome an inadvertent loss of structure in an EFOV image by reversing the 25 scanhead direction, reacquiring the desired structure in the image by realigning the scanhead with the vessel structure, and continuing the EFOV scan without having to start from the beginning.

Claims

35 1. A method of ultrasonic diagnostic imaging that produces an extended field of view image (80) from a plurality of partially spatially overlapping elemental images (A, B, C) acquired by moving a scanhead (10) along the body (94) of a patient in a first motion direction (14a) and in a second motion direction (14b), which is substantially opposite to said first motion direction,

40 the method comprising the steps of:

45 storing elemental images in an image buffer (42; 130), whereby a new elemental image (C) is stored in an aligned position with respect to a previous elemental image (B), whereby the new elemental image is offset from the previous elemental image in a first coordinate direction or in a second coordinate direction which is substantially the reverse of said first coordinate direction, depending on whether the scanhead moves in the first motion direction (14a) or in the second motion direction (14b), respectively; and
removing from said extended field of view image (80) a portion (82) of said previous elemental image that does not spatially overlap said new elemental image when the scanhead moves in the second motion direction (14b), so as to correspondingly reduce the lateral size of said extended field of view image (80).

50 2. A method according to claim 1, the method comprising the step of:

55 substituting the portion (82) that has been removed from said extended field of view image (80) by at least a portion (72) of a new elemental image when the scanhead (10) moves in a third motion direction (14d) that is substantially opposite to said second motion direction (14b).

3. An ultrasonic diagnostic imaging system for producing an extended field of view image (80) from a plurality of partially spatially overlapping elemental images (A, B, C) acquired by moving a scanhead (10) along the body (94) of a

patient in a first motion direction (14a) and in a second motion direction (14b), which is substantially opposite to said first motion direction,
the ultrasonic diagnostic imaging system comprising:

5 an image buffer (42; 130) for storing elemental images;
 means (40) for storing in said buffer a new elemental image (C) in an aligned position with respect to a previous elemental image (B), whereby the new elemental image is offset from the previous elemental image in a first coordinate direction or in a second coordinate direction which is substantially the reverse of said first coordinate direction, depending on whether the scanhead moves in the first motion direction (14a) or in the second motion direction (14b), respectively; and
 10 means (40) for removing from said extended field of view image (80) a portion (82) of said previous elemental image that does not spatially overlap said new elemental image when the scanhead moves in the second motion direction (14b), so as to correspondingly reduce the lateral size of said extended field of view image (80).

15 4. An ultrasonic diagnostic imaging system according to claim 3, comprising:

means (40) for substituting the portion (82) that has been removed from said extended field of view image (80) by at least a portion (72) of a new elemental image when the scanhead moves in a third motion direction (14d) 20 that is substantially opposite to said second motion direction (14b).

Patentansprüche

1. Verfahren der diagnostischen Ultraschallbildgebung, das ein Bild (80) mit einem erweiterten Blickfeld erzeugt aus einer Vielzahl von sich teilweise räumlich überlappenden elementaren Bildern (A, B, C), die erfasst werden, indem ein Schallkopf (10) längs des Körpers (94) eines Patienten in einer ersten Bewegungsrichtung (14a) und einer zweiten, der ersten Bewegungsrichtung im Wesentlichen entgegengesetzten Bewegungsrichtung (14b) bewegt wird, wobei das Verfahren die folgenden Schritte umfasst:

30 Speichern von elementaren Bildern in einem Bildpuffer (42; 130), wobei ein neues elementares Bild (C) in einer ausgerichteten Position in Bezug auf ein vorheriges elementares Bild (B) gespeichert wird, wobei das neue elementare Bild zu dem vorherigen elementaren Bild in einer ersten Koordinatenrichtung oder in einer zweiten Koordinatenrichtung versetzt ist, die im Wesentlichen umgekehrt zur genannten ersten Koordinatenrichtung verläuft, in Abhängigkeit davon, ob sich der Schallkopf in der ersten Bewegungsrichtung (14a) bzw. der zweiten Bewegungsrichtung (14b) bewegt, und

35 Entfernen aus dem genannten Bild (80) mit erweitertem Blickfeld eines Teilstücks (82) des genannten vorherigen elementaren Bildes, das sich nicht räumlich mit dem genannten neuen elementaren Bild überlappt, wenn sich der Schallkopf in der zweiten Bewegungsrichtung (14b) bewegt, um die seitliche Größe des Bildes (80) mit erweitertem Blickfeld entsprechend zu reduzieren.

40 2. Verfahren nach Anspruch 1, das folgenden Schritt umfasst:

Ersetzen des Teilstückes (82), das aus dem genannten Bild (80) mit erweitertem Blickfeld entfernt wurde, durch mindestens ein Teilstück (72) eines neuen elementaren Bildes, wenn sich der Schallkopf (10) in eine dritte Bewegungsrichtung (14d) bewegt, die im Wesentlichen entgegengesetzt zu der genannten zweiten Bewegungsrichtung (14b) ist.

45 3. Diagnostisches Ultraschall-Bildgebungssystem zum Erzeugen eines Bildes (80) mit erweitertem Blickfeld aus einer Vielzahl von sich teilweise räumlich überlappenden elementaren Bildern (A, B, C), die erfasst werden, indem ein Schallkopf (10) längs des Körpers (94) eines Patienten in einer ersten Bewegungsrichtung (14a) und einer zweiten, der ersten Bewegungsrichtung im Wesentlichen entgegengesetzten Bewegungsrichtung (14b) bewegt wird, wobei das diagnostische Ultraschall-Bildgebungssystem Folgendes umfasst:

50 einen Bildpuffer (42; 130) zum Speichern von elementaren Bildern,
 Mittel (40) zum Speichern in dem genannten Puffer eines neuen elementaren Bildes (C) in einer ausgerichteten Position in Bezug auf ein vorheriges elementares Bild (B) gespeichert wird, wobei das neue elementare Bild zu dem vorherigen elementaren Bild in einer ersten Koordinatenrichtung oder in einer zweiten Koordinatenrichtung versetzt ist, die im Wesentlichen umgekehrt zur genannten ersten Koordinatenrichtung verläuft, in Abhän-

gigkeit davon, ob sich der Schallkopf in der ersten Bewegungsrichtung (14a) bzw. der zweiten Bewegungsrichtung (14b) bewegt, und
 5 Mittel (40) zum Entfernen aus dem genannten Bild (80) mit erweitertem Blickfeld eines Teilstücks (82) des genannten vorherigen elementaren Bildes, das sich nicht räumlich mit dem genannten neuen elementaren Bild überlappt, wenn sich der Schallkopf in der zweiten Bewegungsrichtung (14b) bewegt, um die seitliche Größe des Bildes (80) mit erweitertem Blickfeld entsprechend zu reduzieren.

4. Diagnostisches Ultraschall-Bildgebungssystem nach Anspruch 3, das Folgendes umfasst:

10 Mittel (40) zum Ersetzen des Teilstückes (82), das aus dem genannten Bild (80) mit erweitertem Blickfeld entfernt wurde, durch mindestens ein Teilstück (72) eines neuen elementaren Bildes, wenn sich der Schallkopf (10) in eine dritte Bewegungsrichtung (14d) bewegt, die im Wesentlichen entgegengesetzt zu der genannten zweiten Bewegungsrichtung (14b) ist.

15 **Revendications**

1. Procédé d'imagerie diagnostique à ultrasons qui produit une image à champ de vision étendu (80) à partir d'une pluralité d'images élémentaires se superposant partiellement dans l'espace (A, B, C) acquises en déplaçant une tête de balayage (10) le long du corps (94) d'un patient dans une première direction de mouvement (14a) et dans une deuxième direction de mouvement (14b) qui est pratiquement opposée à ladite première direction de mouvement,
 20 le procédé comportant en outre les étapes suivantes :

25 stockage des images élémentaires dans une mémoire tampon d'image (42;130), par lequel une nouvelle image élémentaire (C) est stockée dans une position alignée par rapport à une image élémentaire précédente (B), par lequel la nouvelle image élémentaire est décalée de l'image élémentaire précédente dans la direction d'une première coordonnée ou dans la direction d'une deuxième coordonnée qui est pratiquement l'inverse de ladite première direction de coordonnée, selon que la tête de balayage se déplace dans la première direction de mouvement (14a) ou dans la deuxième direction de mouvement (14b), respectivement; et
 30 effacement dans ladite image à champ de vision étendu (80) d'une portion (82) de ladite image élémentaire précédente qui ne se superpose pas dans l'espace à ladite nouvelle image élémentaire quand la tête de balayage se déplace dans la deuxième direction de mouvement (14b), afin de réduire en conséquence la taille latérale de ladite image à champ de vision étendu (80).

35 2. Procédé selon la revendication 1, le procédé comportant l'étape de:

40 substitution de la portion (82) qui a été effacée de ladite image à champ de vision étendu (80) par au moins une portion (72) d'une nouvelle image élémentaire quand la tête de balayage (10) se déplace dans une troisième direction de mouvement (14d) qui est pratiquement opposée à ladite deuxième direction de mouvement (14b).

45 3. Système d'imagerie diagnostique à ultrasons permettant de produire une image à champ de vision étendu (80) à partir d'une pluralité d'images élémentaires se superposant partiellement dans l'espace (A, B, C) acquises en déplaçant une tête de balayage (10) le long du corps (94) d'un patient dans une première direction de mouvement (14a) et dans une deuxième direction de mouvement (14b) qui est pratiquement opposée à ladite première direction de mouvement,
 le système d'image diagnostique à ultrasons comportant:

50 une mémoire tampon d'images (42; 130) permettant de stocker les images élémentaires; un moyen (40) permettant de stocker dans ladite mémoire tampon une nouvelle image élémentaire (C) dans une position alignée par rapport à une image élémentaire précédente (B), la nouvelle image élémentaire étant décalée de l'image élémentaire précédente dans une première direction de coordonnée ou dans une deuxième direction de coordonnée qui est pratiquement l'inverse de ladite première direction de coordonnée, selon que la tête de balayage se déplace dans la première direction de mouvement (14a) ou dans la deuxième direction de mouvement (14b), respectivement; et
 55 un moyen (40) permettant d'effacer de ladite image à champ de vision étendu (80) une portion (82) de ladite image élémentaire précédente qui ne se superpose pas dans l'espace à ladite nouvelle image élémentaire quand la tête de balayage se déplace dans la deuxième direction de mouvement (14b), afin de réduire en

conséquence la taille latérale de ladite image à champ de vision étendu (80).

4. Système d'imagerie diagnostique à ultrasons selon la revendication 3, comportant:

5 un moyen (40) permettant de substituer la portion (82) qui a été enlevée de ladite image à champ de vision étendu (80) par au moins une portion (72) d'une nouvelle image élémentaire quand la tête de balayage se déplace dans une troisième direction de mouvement (14d) qui est pratiquement opposée à ladite deuxième direction de mouvement (14b).

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FIG. 1

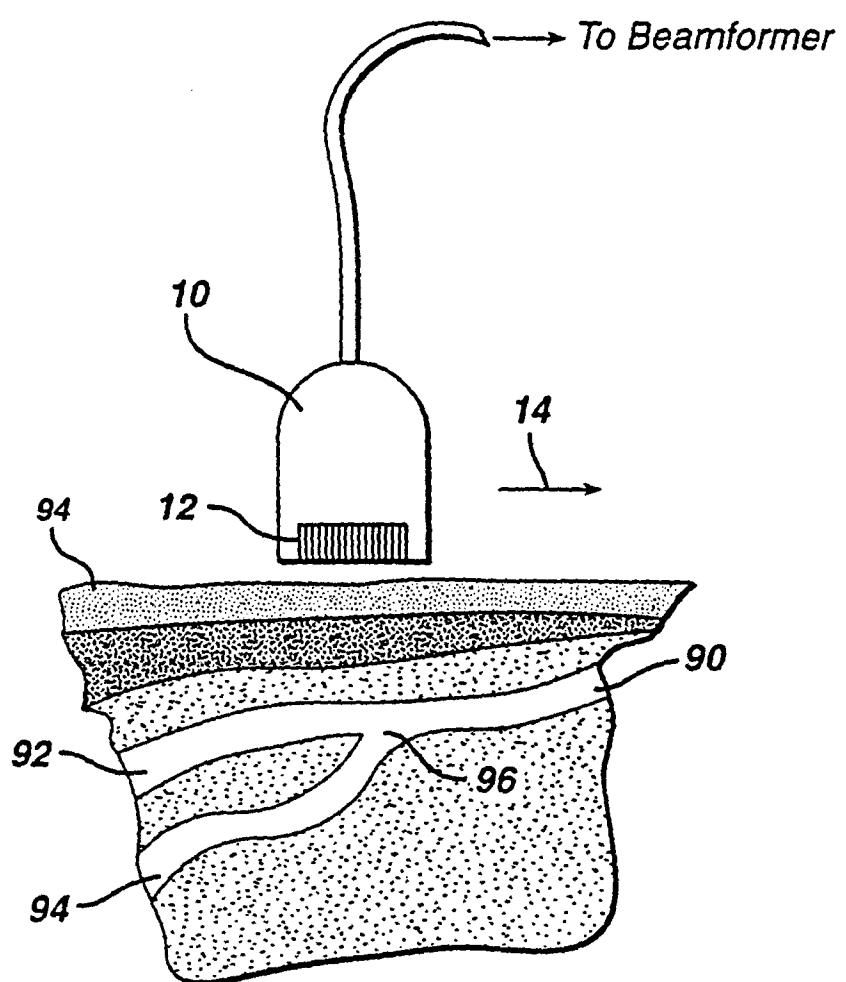
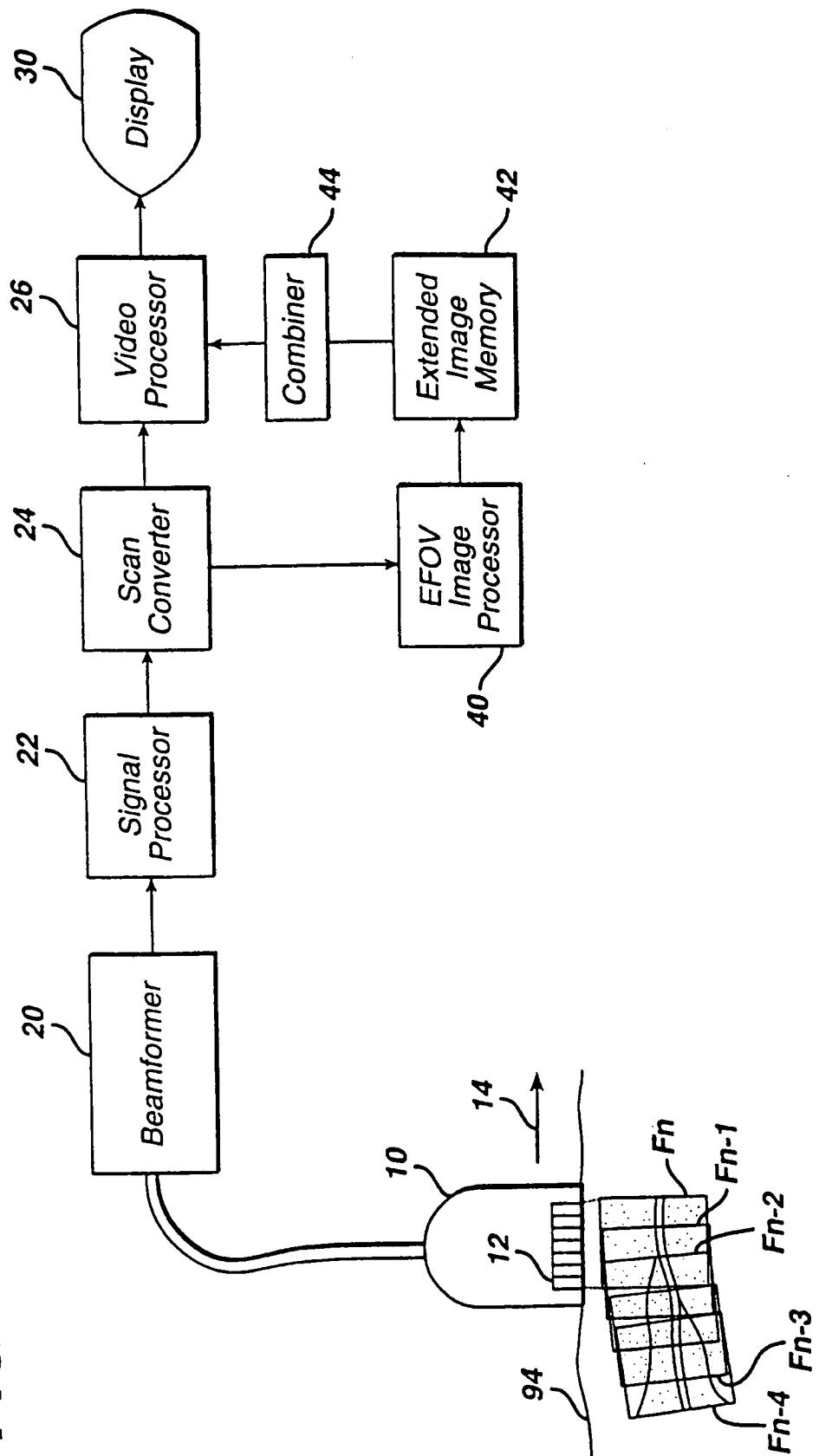


FIG. 2



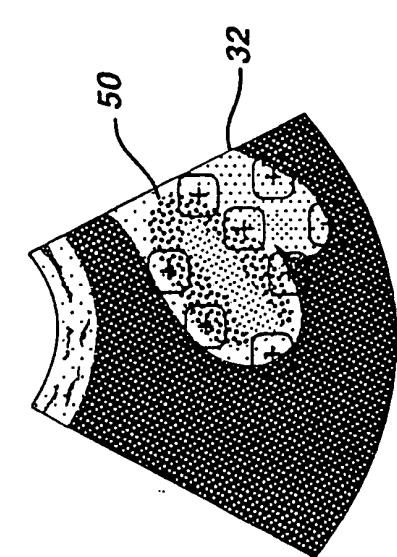


FIG. 3a

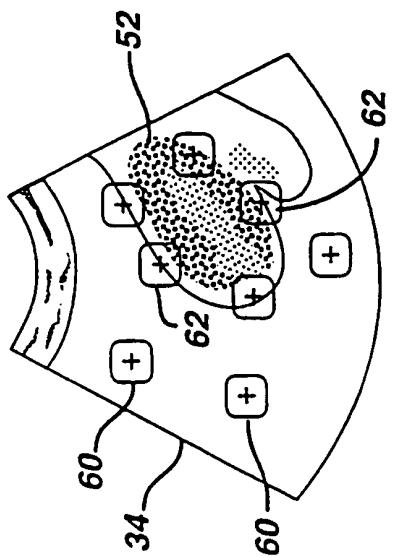


FIG. 3b

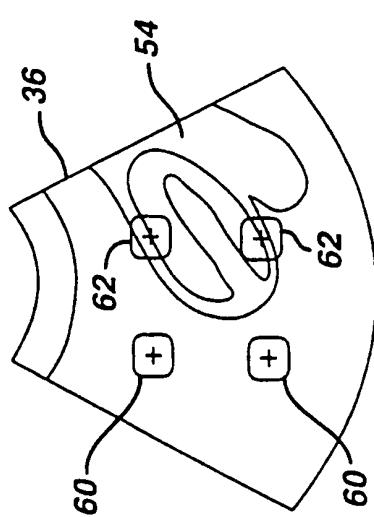


FIG. 3c

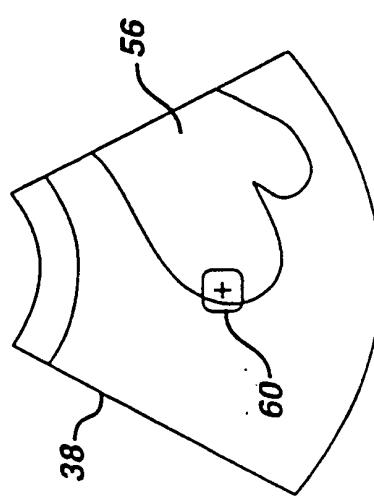


FIG. 3d

FIG. 4a

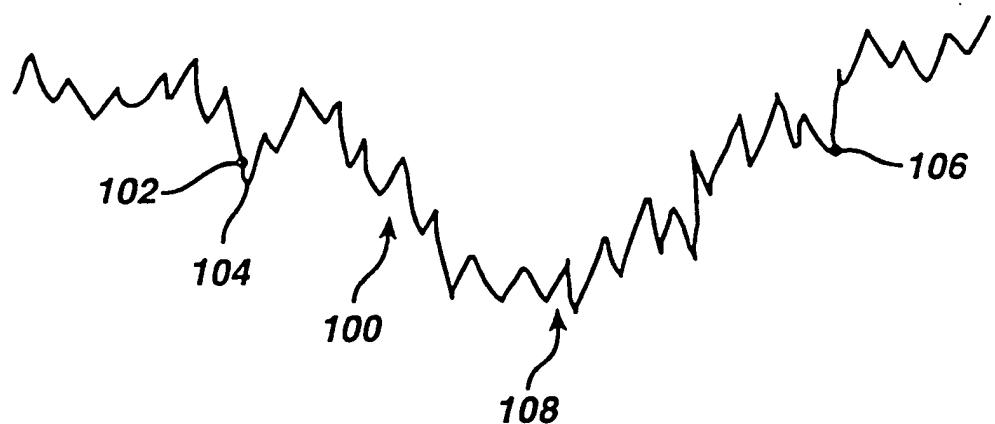


FIG. 4b

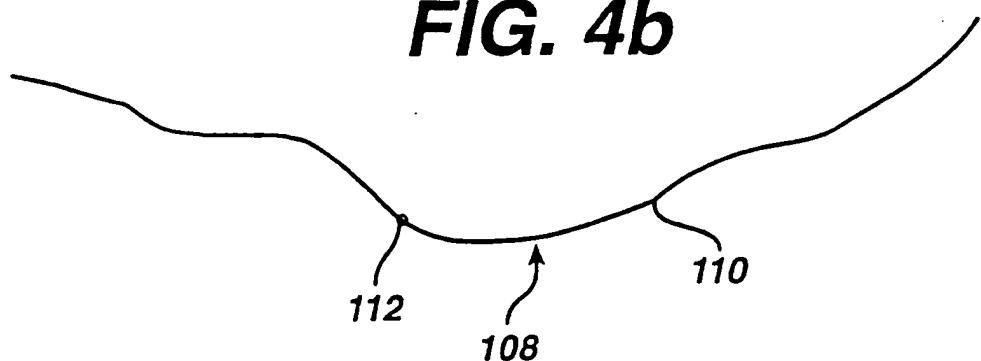


FIG. 4c

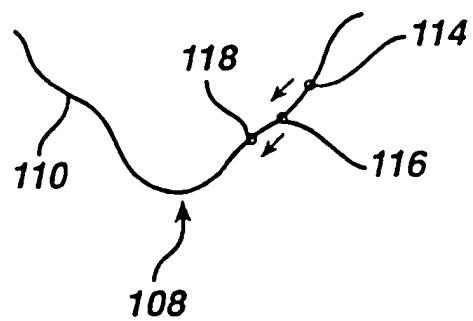


FIG. 5a

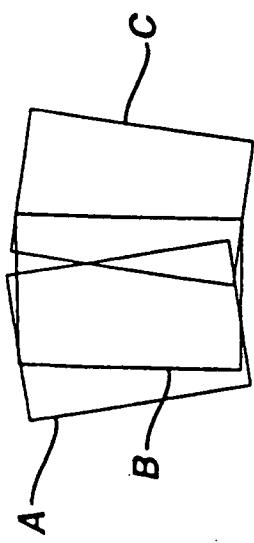


FIG. 5b

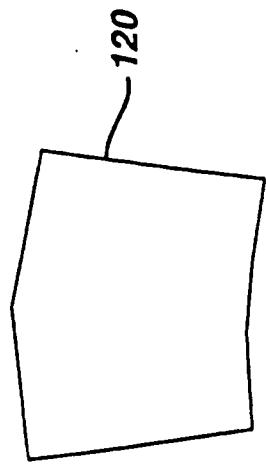


FIG. 6

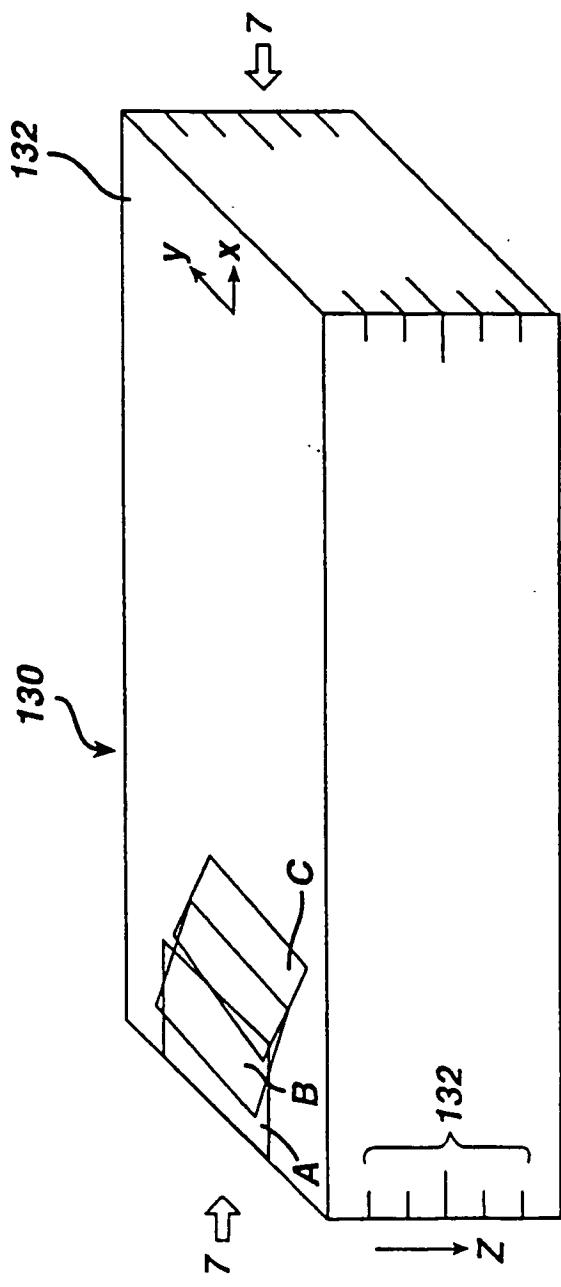


FIG. 7a

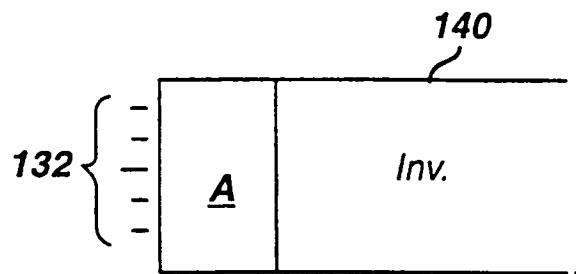


FIG. 7b

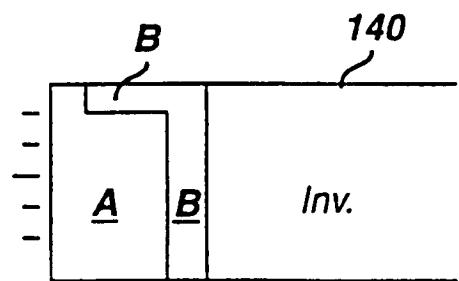


FIG. 7c

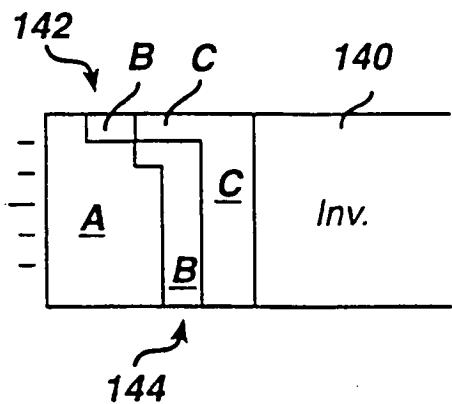


FIG. 8a

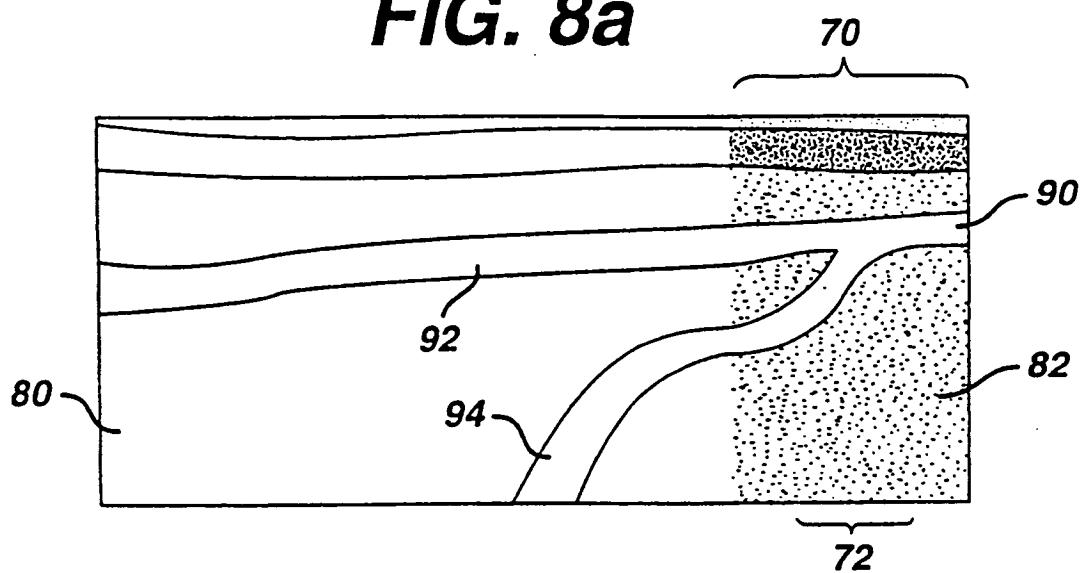


FIG. 8b

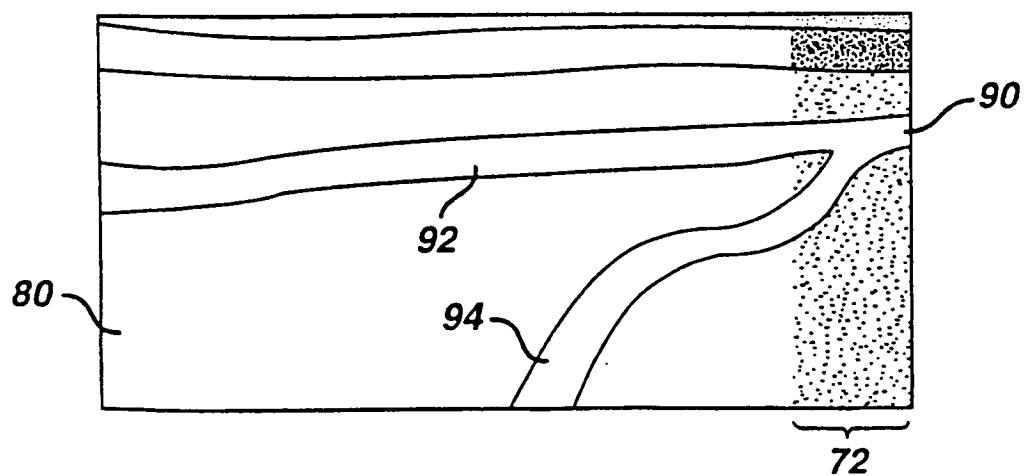


FIG. 9a

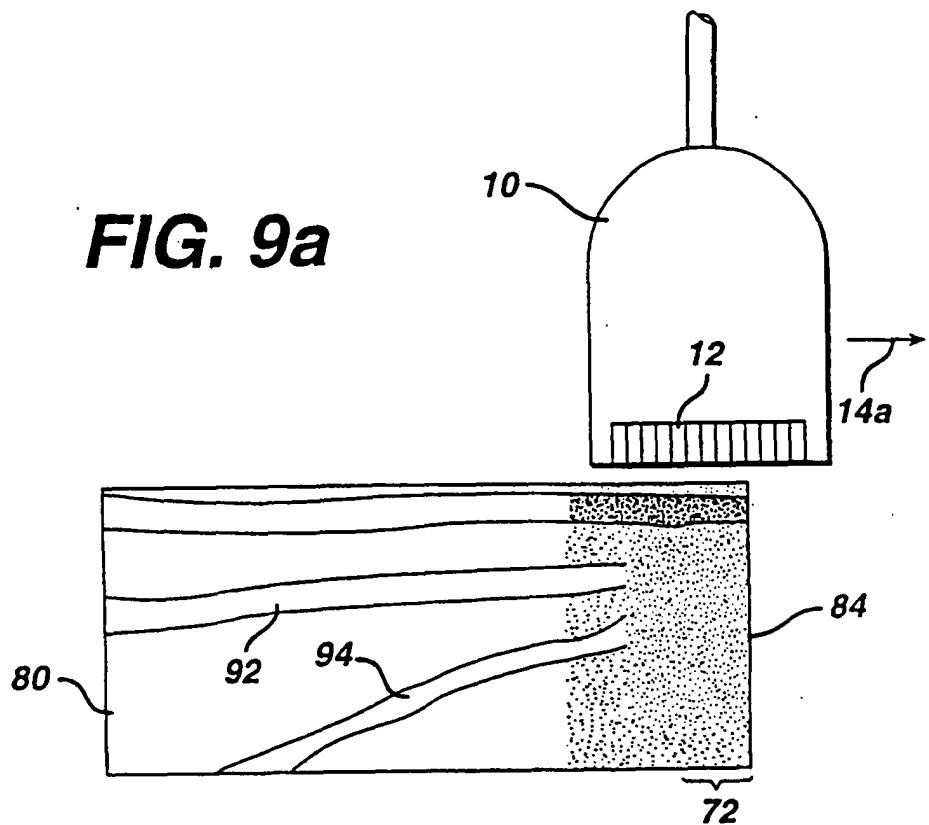


FIG. 9b

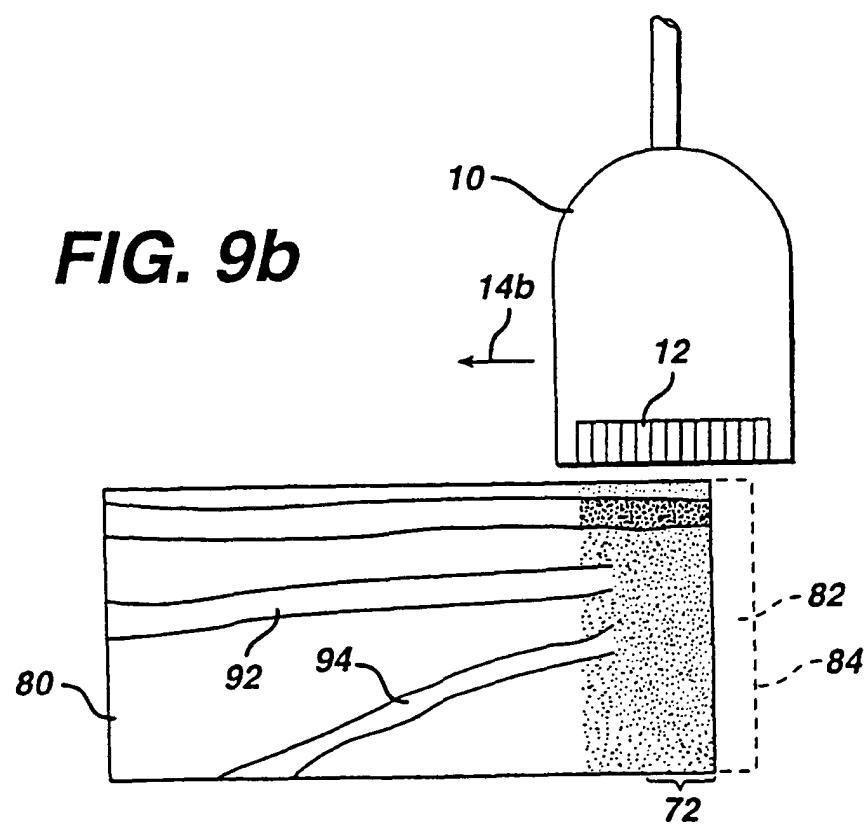


FIG. 9c

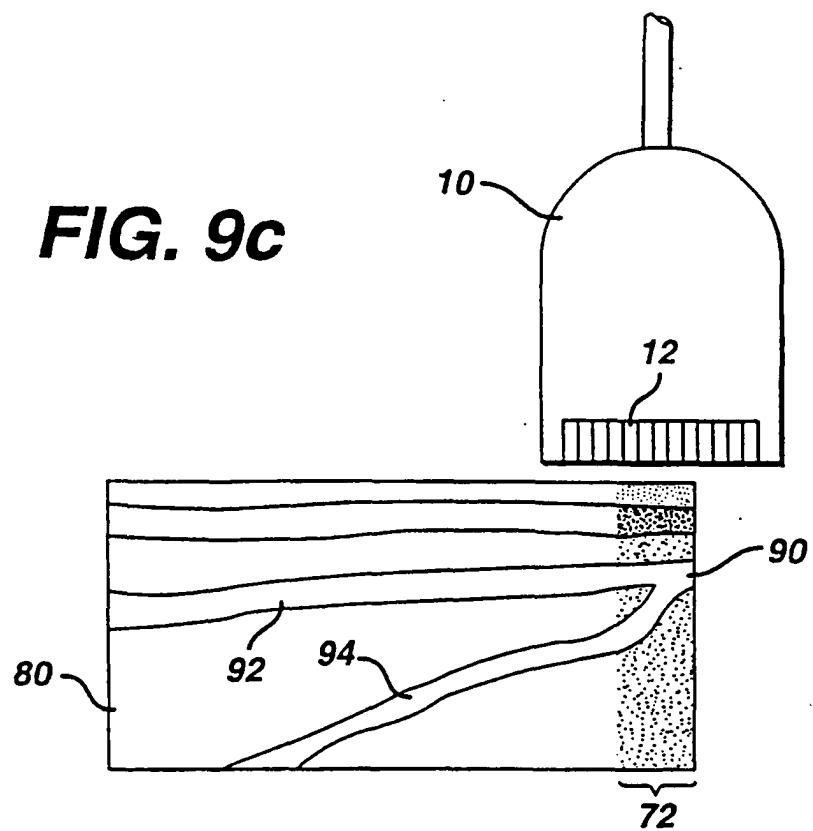


FIG. 9d

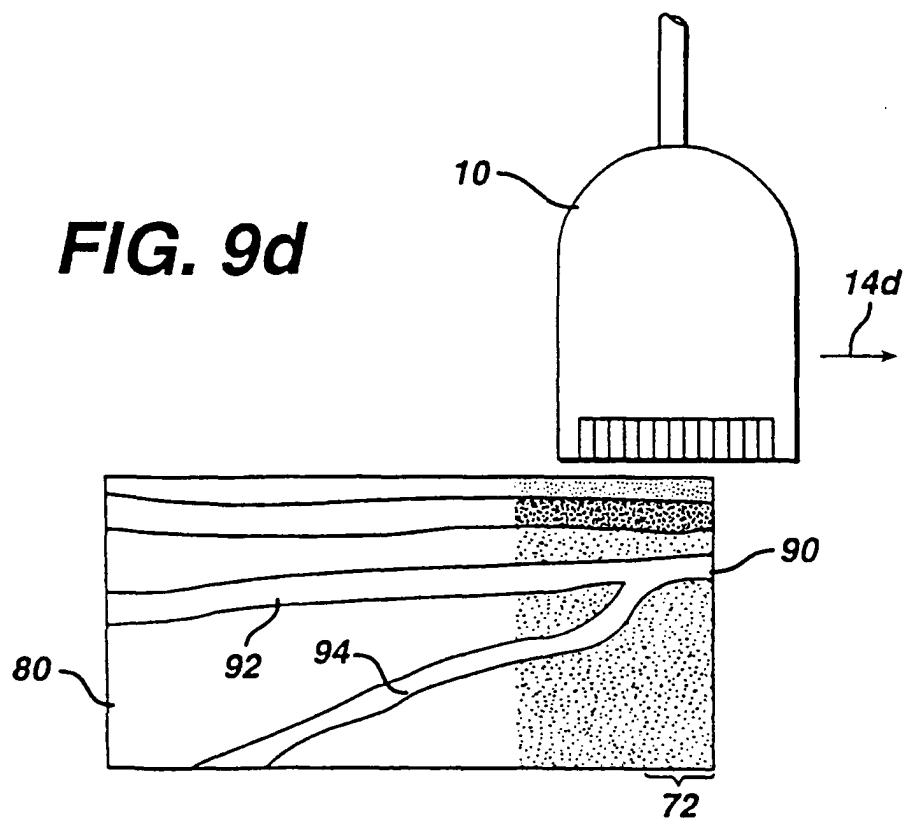
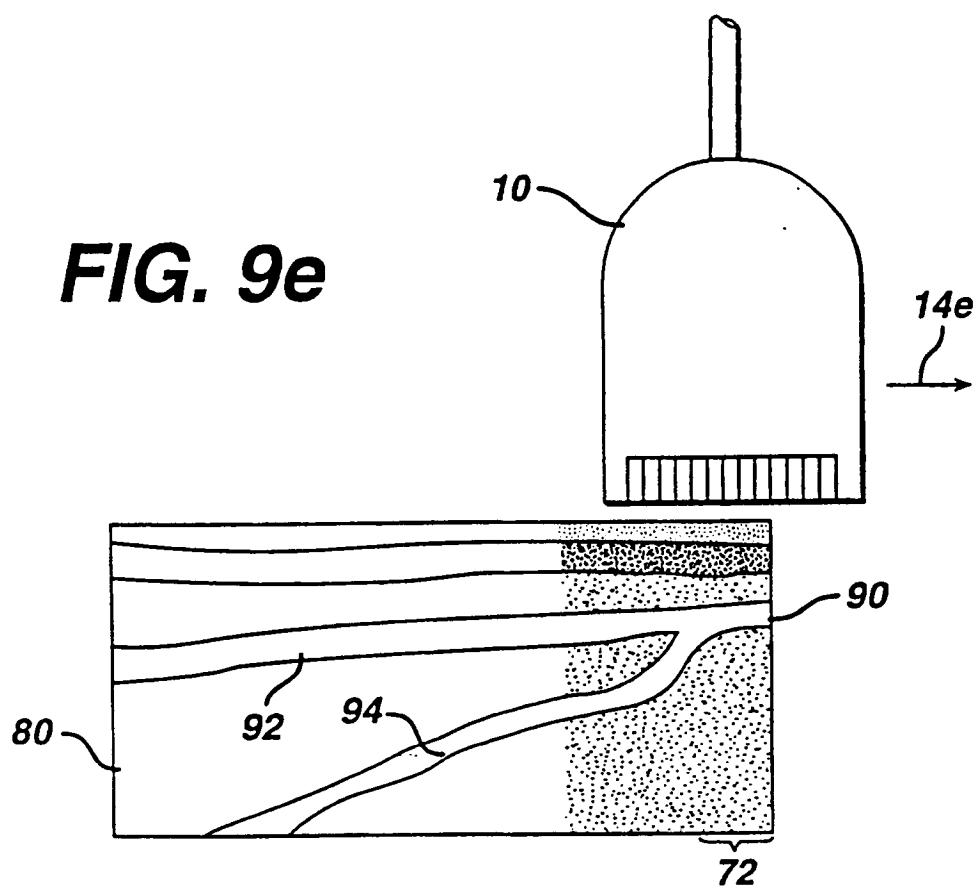


FIG. 9e



REFERENCES CITED IN THE DESCRIPTION

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Patent documents cited in the description

- US 5566674 A [0015]

Non-patent literature cited in the description

- **Y. HARA et al.** A New Sonographic Technique for Assessing Carotid Artery Disease: Extended-Field-of-View Imaging. *the American Journal of Neuroradiology*, February 1999, vol. 20, 267-270 [0003]

专利名称(译)	具有图像重新获取的扩展视野超声诊断成像		
公开(公告)号	EP1107697B1	公开(公告)日	2008-02-27
申请号	EP2000940404	申请日	2000-06-26
[标]申请(专利权)人(译)	皇家飞利浦电子股份有限公司		
申请(专利权)人(译)	皇家飞利浦电子N.V.		
当前申请(专利权)人(译)	皇家飞利浦电子N.V.		
[标]发明人	PETERSON ROY B WISSLER THOMAS M OLSSON LARS J		
发明人	PETERSON, ROY, B. WISSLER, THOMAS, M. OLSSON, LARS, J.		
IPC分类号	A61B8/00 A61B8/08 A61B8/14 A61B8/06 H04N1/387		
CPC分类号	G01S7/52065 A61B8/08 A61B8/463 A61B8/5253 G01S7/5205		
优先权	09/345242 1999-06-30 US		
其他公开文献	EP1107697A1		
外部链接	Espacenet		

摘要(译)

当扫描头的移动偏离期望的行进路径时，扩展的视野超声成像系统允许反转扫描头运动的方向以重新获得期望的图像平面或患者解剖结构。

$$\sum_{y=0}^8 \sum_{x=0}^8 |P_{N(x-x-dx, y-y-dy)} - P_{O(x-x, y-y)}|$$