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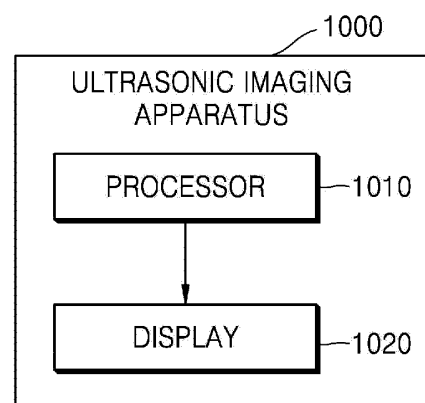
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(54) **ULTRASONIC IMAGING DEVICE AND ULTRASONIC IMAGE DISPLAY METHOD**

(57) Provided are an ultrasonic imaging apparatus and a method of displaying an ultrasound image. The ultrasonic imaging apparatus may include: a processor configured to acquire a Doppler signal corresponding to a sample volume, divide the Doppler signal into a plurality of sub-Doppler signals, generate a plurality of spectral Doppler signals by performing spectral analysis on each of the plurality of sub-Doppler signals, and generate, from the plurality of spectral Doppler signals, a spectral Doppler signal corresponding to the sample volume; and a display displaying the spectral Doppler signal corresponding to the sample volume.

FIG. 3



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Description

TECHNICAL FIELD

5 **[0001]** The present disclosure relates to an ultrasonic imaging apparatus for generating and displaying a spectral Doppler signal and a method of displaying an ultrasound image.

BACKGROUND ART

10 **[0002]** Ultrasonic imaging apparatuses generate ultrasound signals for a predetermined inner region of an object via a probe and use information of reflected echo signals to obtain an image of the inner region of the object. In particular, ultrasonic imaging apparatuses are used for medical purposes including observation, assessment of injuries, and detection of foreign substances inside an object. Such ultrasonic imaging apparatuses exhibit high stability, display images in real time, and are safe due to lack of radiation exposure compared to diagnostic X-ray apparatuses. Therefore,

15 **[0003]** Furthermore, ultrasonic imaging apparatuses have been widely used together with other types of imaging diagnosis apparatuses. **[0003]** Furthermore, ultrasonic imaging apparatuses may provide a Doppler image showing movement of an object to a user. In other words, ultrasonic imaging apparatuses may measure and output movement of the object by using various Doppler images such as color Doppler, spectral Doppler, and vector Doppler images.

20 DESCRIPTION OF EMBODIMENTS

TECHNICAL PROBLEM

25 **[0004]** Provided are an ultrasonic imaging apparatus for generating and displaying a spectral Doppler signal and a method of displaying an ultrasound image.

SOLUTION TO PROBLEM

30 **[0005]** According to an aspect of the present disclosure, an ultrasonic imaging apparatus may include: a processor configured to acquire a Doppler signal corresponding to a sample volume, divide the Doppler signal into a plurality of sub-Doppler signals, generate a plurality of spectral Doppler signals by performing spectral analysis on each of the plurality of sub-Doppler signals, and generate a spectral Doppler signal corresponding to the sample volume, based on the plurality of spectral Doppler signals; and a display displaying the spectral Doppler signal corresponding to the sample volume.

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ADVANTAGEOUS EFFECTS OF DISCLOSURE

40 **[0006]** According to some embodiments, an ultrasonic imaging apparatus may divide a Doppler signal corresponding to a sample volume into a plurality of sub-Doppler signals and generate a spectral Doppler signal corresponding to the sample volume based on a plurality of spectral Doppler signals respectively corresponding to the plurality of sub-Doppler signals. Thus, it is possible to display the spectral Doppler signal corresponding to the sample volume as a high-quality image.

BRIEF DESCRIPTION OF DRAWINGS

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[0007]

FIG. 1 is a block diagram of a configuration of an ultrasound diagnosis apparatus according to an embodiment.

FIGS. 2A through 2C illustrate ultrasound diagnosis apparatuses according to embodiments.

50 FIG. 3 is a block diagram of an ultrasonic imaging apparatus according to an embodiment.

FIG. 4 is a diagram illustrating an embodiment in which an ultrasonic imaging apparatus generates a spectral Doppler signal corresponding to a sample volume.

FIG. 5 is a diagram illustrating a detailed embodiment in which an ultrasonic imaging apparatus generates a spectral Doppler signal corresponding to a sample volume.

55 FIG. 6 is a diagram illustrating an embodiment in which an ultrasonic imaging apparatus generates a spectral Doppler signal corresponding to a sample volume.

FIG. 7 is a flowchart of a method by which an ultrasonic imaging apparatus displays an ultrasound image, according to an embodiment.

FIG. 8 is a block diagram of an ultrasonic imaging apparatus according to another embodiment.

FIG. 9 illustrates an embodiment in which an ultrasonic imaging apparatus displays a plurality of spectral Doppler signals.

FIG. 10 illustrates an embodiment in which an ultrasonic imaging apparatus displays a plurality of spectral Doppler signals as a single image.

FIG. 11 illustrates an embodiment in which an ultrasonic imaging apparatus displays a plurality of spectral Doppler signals.

FIG. 12 illustrates an embodiment in which an ultrasonic imaging apparatus provides information about vascular wall stiffness.

FIG. 13 illustrates an embodiment in which an ultrasonic imaging apparatus displays a plurality of spectral Doppler signals.

FIG. 14 illustrates a method by which an ultrasonic imaging apparatus displays an ultrasound image, according to an embodiment.

FIG. 15 is a block diagram of an ultrasonic imaging apparatus according to another embodiment.

FIG. 16 illustrates an embodiment in which an ultrasonic imaging apparatus generates a spectral Doppler signal corresponding to an object.

FIG. 17 illustrates a detailed embodiment in which an ultrasonic imaging apparatus generates a spectral Doppler signal corresponding to an object.

FIG. 18 illustrates another embodiment in which an ultrasonic imaging apparatus generates a spectral Doppler signal corresponding to an object.

FIG. 19 is a flowchart of a method by which an ultrasonic imaging apparatus displays an ultrasound image, according to an embodiment.

BEST MODE

[0008] According to an embodiment, an ultrasonic imaging apparatus may include: a processor configured to acquire a Doppler signal corresponding to a sample volume, divide the Doppler signal into a plurality of sub-Doppler signals, generate a plurality of spectral Doppler signals by performing spectral analysis on each of the plurality of sub-Doppler signals, and generate, from the plurality of spectral Doppler signals, a spectral Doppler signal corresponding to the sample volume; and a display displaying the spectral Doppler signal corresponding to the sample volume.

[0009] According to an embodiment, the processor may generate the plurality of spectral Doppler signals by performing weighting accumulation and Fourier Transform on each of the plurality of sub-Doppler signals.

[0010] According to an embodiment, the processor may perform weighting accumulation by using a predetermined window function.

[0011] According to an embodiment, the processor may acquire the Doppler signal every period according to a pulse repetition frequency (PRF).

[0012] According to an embodiment, the processor may generate the spectral Doppler signal corresponding to the sample volume by performing weighting accumulation on the plurality of spectral Doppler signals.

[0013] According to an embodiment, the processor may divide the Doppler signal into the plurality of sub-Doppler signals respectively corresponding to a plurality of sections set in the sample volume.

[0014] According to an embodiment, the number and length of the plurality of sections may be set based on a user input.

[0015] According to an embodiment, the processor may determine at least one effective spectral Doppler signal from among the plurality of spectral Doppler signals and generate the spectral Doppler signal corresponding to the sample volume from the determined at least one spectral Doppler signal.

[0016] According to an embodiment, the ultrasonic imaging apparatus may further include an ultrasound transceiver configured to control a probe to transmit a generated ultrasound signal to the sample volume as many times as a predetermined ensemble number and according to a preset PRF, and receive an echo signal reflected from the sample volume, and the processor may acquire the Doppler signal based on the echo signal.

[0017] According to an embodiment, a method of displaying an ultrasound image may include: acquiring a Doppler signal corresponding to a sample volume; dividing the Doppler signal into a plurality of sub-Doppler signals; generating a plurality of spectral Doppler signals by performing spectral analysis on each of the plurality of sub-Doppler signals; generating, from the plurality of spectral Doppler signals, a spectral Doppler signal corresponding to the sample volume; and displaying the spectral Doppler signal corresponding to the sample volume.

[0018] According to an embodiment, an ultrasonic imaging apparatus may include: a processor configured to acquire a Doppler signal corresponding to a sample volume, divide the Doppler signal into a plurality of sub-Doppler signals respectively corresponding to a plurality of sections set in the sample volume, and generate a plurality of spectral Doppler signals respectively corresponding to the plurality of sections by performing spectral analysis on each of the plurality of sub-Doppler signals; and a display displaying the plurality of spectral Doppler signals.

[0019] According to an embodiment, the processor may generate a plurality of spectral lines respectively corresponding to a plurality of sections by performing line tracing on the respective plurality of spectral Doppler signals, and the display may display the plurality of spectral lines.

[0020] According to an embodiment, when the sample volume is set with respect to a blood vessel, the processor may generate information about vascular wall stiffness based on the plurality of spectral Doppler signals, and the display may display the information about vascular wall stiffness.

[0021] According to an embodiment, the processor may respectively detect peak systolic velocities (PSVs) for the plurality of sections based on the plurality of spectral Doppler signals and generate information about vascular wall stiffness based on the PSVs for the plurality of sections.

[0022] According to an embodiment, when the sample volume is set with respect to an object, the processor may select at least one spectral Doppler signal representing the object from among the plurality of spectral Doppler signals, and the display may display the selected at least one spectral Doppler signal.

[0023] According to an embodiment, the ultrasonic imaging apparatus may further include a user input interface that receives an input of selecting at least one spectral Doppler signal representing the object from a user.

[0024] According to an embodiment, the object may be a microscopic blood vessel.

[0025] According to an embodiment, the number and length of the plurality of sections may be set based on a user input.

[0026] According to an embodiment, the processor may generate the plurality of spectral Doppler signals by respectively performing weighting accumulation and Fourier Transformation on the plurality of sub-Doppler signals.

[0027] According to an embodiment, a method of displaying an ultrasound image may include: acquiring a Doppler signal corresponding to a sample volume; dividing the Doppler signal into a plurality of sub-Doppler signals respectively corresponding to a plurality of sections set in the sample volume; generating a plurality of spectral Doppler signals respectively corresponding to the plurality of sections by performing spectral analysis on each of the plurality of sub-Doppler signals; and displaying the plurality of spectral Doppler signals.

[0028] According to an embodiment, an ultrasonic imaging apparatus may include: a processor configured to acquire a Doppler signal corresponding to a sample volume set with respect to an object, generate a plurality of spectral Doppler signals respectively corresponding to a plurality of sections set in the sample volume by performing spectral analysis on each of the Doppler signal from the plurality of sections, model an artifact signal in a spectral Doppler signal corresponding to the object by using the plurality of spectral Doppler signals, and generate, based on the spectral Doppler signal corresponding to the object and the artifact signal, a spectral Doppler signal corresponding to the object and from which an artifact is removed; and a display displaying the spectral Doppler signal corresponding to the object and from which the artifact is removed.

[0029] According to an embodiment, the processor may determine a spectral Doppler signal corresponding to a section including the object from among the plurality of sections as the spectral Doppler signal corresponding to the object.

[0030] According to an embodiment, the processor may determine as an artifact signal an ultrasound reflected signal from another object, which is contained in the spectral Doppler signal corresponding to the object and model the artifact signal by using a spectral Doppler signal corresponding to a section including the other object from among the plurality of sections.

[0031] According to an embodiment, the object may correspond to a vein while the other object may correspond to an artery.

[0032] According to an embodiment, the processor may generate the spectral Doppler signal corresponding to the object and from which the artifact is removed by performing subtraction between the spectral Doppler signal corresponding to the object and the artifact signal.

[0033] According to an embodiment, the processor may divide the Doppler signal into a plurality of sub-Doppler signals respectively corresponding to the plurality of sections and generate the plurality of spectral Doppler signals by performing spectral analysis on each of the plurality of sub-Doppler signals.

[0034] According to an embodiment, the ultrasonic imaging apparatus may further include an ultrasound transceiver configured to control a probe to transmit ultrasound signals along a pulsed Doppler line passing through the sample volume set with respect to the object and receive echo signals reflected from the sample volume and at least one volume on the pulsed Doppler line. The processor may acquire from the received echo signals a Doppler signal corresponding to the sample volume and at least one Doppler signal corresponding to the at least one volume, generate a spectral Doppler signal corresponding to the object and at least one spectral Doppler signal by performing spectral analysis on each of the Doppler signal corresponding to the sample volume and the at least one Doppler signal, model an artifact signal in the spectral Doppler signal corresponding to the object by using the at least one spectral Doppler signal, and generate, based on the spectral Doppler signal corresponding to the object and the artifact signal, a spectral Doppler signal corresponding to the object and from which an artifact is removed.

[0035] According to an embodiment, a method of displaying an ultrasound image may include: acquiring a Doppler signal corresponding to a sample volume set with respect to an object; generating a plurality of spectral Doppler signals respectively corresponding to a plurality of sections set in the sample volume by performing spectral analysis on the

Doppler signal in each of the plurality of sections; modeling an artifact signal in a spectral Doppler signal corresponding to the object by using the plurality of spectral Doppler signals; generating, based on the spectral Doppler signal corresponding to the object and the artifact signal, a spectral Doppler signal corresponding to the object and from which an artifact is removed; and displaying the spectral Doppler signal corresponding to the object and from which the artifact is removed.

MODE OF DISCLOSURE

[0036] The present specification describes principles of the present disclosure and sets forth embodiments thereof to clarify the scope of the present disclosure and to allow those of ordinary skill in the art to implement the embodiments. The present embodiments may have different forms.

[0037] Like reference numerals refer to like elements throughout. The present specification does not describe all components in the embodiments, and common knowledge in the art or the same descriptions of the embodiments will be omitted below. The term "part" or "portion" may be implemented using hardware or software, and according to embodiments, one "part" or "portion" may be formed as a single unit or element or include a plurality of units or elements. Hereinafter, the principles and embodiments of the present disclosure will be described in detail with reference to the accompanying drawings.

[0038] In exemplary embodiments, an image may include any medical image acquired by various medical imaging apparatuses such as a magnetic resonance imaging (MRI) apparatus, a computed tomography (CT) apparatus, an ultrasound imaging apparatus, or an X-ray apparatus.

[0039] Also, in the present specification, an "object", which is a thing to be imaged, may include a human, an animal, or a part thereof. For example, an object may include a part of a human, that is, an organ, blood vessel or a tissue, or a phantom.

[0040] Throughout the specification, an ultrasound image refers to an image of an object processed based on ultrasound signals transmitted to the object and reflected therefrom.

[0041] FIG. 1 is a block diagram illustrating a configuration of an ultrasound diagnosis apparatus 100, i.e., a diagnostic apparatus, according to an exemplary embodiment.

[0042] Referring to FIG. 1, the ultrasound diagnosis apparatus 100 may include a probe 20, an ultrasound transceiver 110, a controller 120, an image processor 130, one or more displays 140, a storage 150, e.g., a memory, a communication module 160, i.e., a communication device or an interface, and an input interface 170.

[0043] The ultrasound diagnosis apparatus 100 may be of a cart-type or a portable-type ultrasound diagnosis apparatus, that is portable, moveable, mobile, or hand-held. Examples of the portable-type ultrasound diagnosis apparatus 100 may include a smart phone, a laptop computer, a personal digital assistant (PDA), and a tablet personal computer (PC), each of which may include a probe and a software application, but embodiments are not limited thereto.

[0044] The probe 20 may include a plurality of transducers. The plurality of transducers may transmit ultrasound signals to an object 10 in response to transmitting signals received by the probe 20, from a transmitter 113. The plurality of transducers may receive ultrasound signals reflected from the object 10 to generate reception signals. In addition, the probe 20 and the ultrasound diagnosis apparatus 100 may be formed in one body (e.g., disposed in a single housing), or the probe 20 and the ultrasound diagnosis apparatus 100 may be formed separately (e.g., disposed separately in separate housings) but linked wirelessly or via wires. In addition, the ultrasound diagnosis apparatus 100 may include one or more probes 20 according to embodiments.

[0045] The controller 120 may control the transmitter 113 for the transmitter 113 to generate transmitting signals to be applied to each of the plurality of transducers based on a position and a focal point of the plurality of transducers included in the probe 20.

[0046] The controller 120 may control the ultrasound receiver 115 to generate ultrasound data by converting reception signals received from the probe 20 from analogue to digital signals and summing the reception signals converted into digital form, based on a position and a focal point of the plurality of transducers.

[0047] The image processor 130 may generate an ultrasound image by using ultrasound data generated from the ultrasound receiver 115. The ultrasound image may be not only a grayscale ultrasound image obtained by scanning an object in an amplitude (A) mode, a brightness (B) mode, and a motion (M) mode, but also a Doppler image representing a moving object by using a Doppler effect. The Doppler image may be a blood flow Doppler image showing flow of blood (also referred to as a color Doppler image), a tissue Doppler image showing a movement of tissue, or a spectral Doppler image showing a moving speed of an object as a waveform. According to an embodiment, the image processor 130 may extract Doppler components from ultrasound data, and may generate a Doppler image showing a movement of an object as colors or waveforms based on the extracted Doppler components.

[0048] The display 140 may display a generated ultrasound image and various pieces of information processed by the ultrasound diagnosis apparatus 100. The ultrasound diagnosis apparatus 100 may include two or more displays 140 according to the present exemplary embodiment. The display 140 may include a touch screen in combination with a

touch panel.

[0049] The controller 120 may control the operations of the ultrasound diagnosis apparatus 100 and flow of signals between the internal elements of the ultrasound diagnosis apparatus 100. The controller 120 may include a memory for storing a program or data to perform functions of the ultrasound diagnosis apparatus 100 and a processor and/or a microprocessor (not shown) for processing the program or data. For example, the controller 120 may control the operation of the ultrasound diagnosis apparatus 100 by receiving a control signal from the input interface 170 or an external apparatus.

[0050] The ultrasound diagnosis apparatus 100 may include the communication module 160 and may be connected to external apparatuses, for example, servers, medical apparatuses, and portable devices such as smart phones, tablet personal computers (PCs), wearable devices, etc., via the communication module 160.

[0051] The communication module 160 may include at least one element capable of communicating with the external apparatuses. For example, the communication module 160 may include at least one among a short-range communication module, a wired communication module, and a wireless communication module.

[0052] The communication module 160 may receive a control signal and data from an external apparatus and transmit the received control signal to the controller 120 so that the controller 120 may control the ultrasound diagnosis apparatus 100 in response to the received control signal.

[0053] The controller 120 may transmit a control signal to the external apparatus via the communication module 160 so that the external apparatus may be controlled in response to the control signal of the controller 120.

[0054] For example, the external apparatus connected to the ultrasound diagnosis apparatus 100 may process the data of the external apparatus in response to the control signal of the controller 120 received via the communication module 160.

[0055] A program for controlling the ultrasound diagnosis apparatus 100 may be installed in the external apparatus. The program may include command languages to perform part of operation of the controller 120 or the entire operation of the controller 120.

[0056] The program may be pre-installed in the external apparatus or may be installed by a user of the external apparatus by downloading the program from a server that provides applications. The server that provides applications may include a recording medium where the program is stored.

[0057] The storage 150 may store various data or programs for driving and controlling the ultrasound diagnosis apparatus 100, input and/or output ultrasound data, ultrasound images, applications, etc.

[0058] The input interface 170 may receive a user's input to control the ultrasound diagnosis apparatus 100 and may include a keyboard, button, keypad, mouse, trackball, jog switch, knob, a touchpad, a touch screen, a microphone, a motion input means, a biometrics input means, etc. For example, the user's input may include inputs for manipulating buttons, keypads, mice, trackballs, jog switches, or knobs, inputs for touching a touchpad or a touch screen, a voice input, a motion input, and a bioinformation input, for example, iris recognition or fingerprint recognition, but an exemplary embodiment is not limited thereto.

[0059] An example of the ultrasound diagnosis apparatus 100 according to the present exemplary embodiment is described below with reference to FIG. 2A, 2B, and 2C.

[0060] FIGS. 2A, 2B, and 2C are diagrams illustrating ultrasound diagnosis apparatus according to an exemplary embodiment.

[0061] Referring to FIGS. 2A and 2B, the ultrasound diagnosis apparatus 100a and 100b may include a main display 121 and a sub-display 122. At least one among the main display 121 and the sub-display 122 may include a touch screen. The main display 121 and the sub-display 122 may display ultrasound images and/or various information processed by the ultrasound diagnosis apparatus 100a and 100b. The main display 121 and the sub-display 122 may provide graphical user interfaces (GUI), thereby receiving user's inputs of data to control the ultrasound diagnosis apparatus 100. For example, the main display 121 may display an ultrasound image and the sub-display 122 may display a control panel to control display of the ultrasound image as a GUI. The sub-display 122 may receive an input of data to control the display of an image through the control panel displayed as a GUI. The ultrasound diagnosis apparatus 100b may control the display of the ultrasound image on the main display 121 by using the input control data.

[0062] Referring to FIG. 2B, the ultrasound diagnosis apparatus 100b may include a control panel 165. The control panel 165 may include buttons, trackballs, jog switches, or knobs, and may receive data to control the ultrasound diagnosis apparatus 100 from the user. For example, the control panel 165 may include a time gain compensation (TGC) button 171 and a freeze button 172. The TGC button 171 is to set a TGC value for each depth of an ultrasound image. Also, when an input of the freeze button 172 is detected during scanning an ultrasound image, the ultrasound diagnosis apparatus 100b may keep displaying a frame image at that time point.

[0063] The buttons, trackballs, jog switches, and knobs included in the control panel 165 may be provided as a GUI to the main display 121 or the sub-display 122.

[0064] Referring to FIG. 2C, the ultrasound diagnosis apparatus 100c may include a portable device. An example of the portable ultrasound diagnosis apparatus 100c may include, for example, smart phones including probes and appli-

cations, laptop computers, personal digital assistants (PDAs), or tablet PCs, but an exemplary embodiment is not limited thereto.

[0065] The ultrasound diagnosis apparatus 100c may include the probe 20 and a main body 40. The probe 20 may be connected to one side of the main body 40 by wire or wirelessly. The main body 40 may include a touch screen 145. The touch screen 145 may display an ultrasound image, various pieces of information processed by the ultrasound diagnosis apparatus 100c, and a GUI.

[0066] FIG. 3 is a block diagram of an ultrasonic imaging apparatus 1000 according to an embodiment.

[0067] The ultrasonic imaging apparatus 1000 may include a processor 1010 and a display 1020. According to an embodiment, the processor 1010 may correspond to at least one or a combination of the image processor 130 and the controller 120 described with reference to FIG. 1, and the display 1020 may correspond to the display 140 of FIG. 1.

[0068] FIG. 3 shows that the ultrasonic imaging apparatus 1000 includes only components related to the present embodiment. Thus, it will be understood by those of ordinary skill in the relevant art that the ultrasonic imaging apparatus 1000 may include other common components as well as the components shown in FIG. 3. For example, the ultrasonic imaging apparatus 1000 may include at least one of the probe 20, the ultrasound transceiver 110, the storage 150, the communication module 160, and the input interface 170 described with reference to FIG. 1.

[0069] The processor 1010 controls all operations of the ultrasonic imaging apparatus 1000 and processes data and signals. The processor 1010 may be composed of at least one hardware unit. According to an embodiment, the processor 1010 may include a separate hardware unit that serves as the image processor 130 and the controller 120. The processor 1010 may be implemented by one or more software modules that are generated by executing program code stored in a memory.

[0070] The processor 1010 may acquire a Doppler signal corresponding to a sample volume. In other words, the processor 1010 may acquire a Doppler signal corresponding to a sample volume set with respect to an object.

[0071] According to an embodiment, the ultrasonic imaging apparatus 1000 may include the ultrasound transceiver 110, and the ultrasound transceiver 110 may control the probe 20 to transmit, to a sample volume, an ultrasound signal which is generated according to a predetermined pulse repetition frequency (PRF) and receive an echo signal reflected from the sample volume. The processor 1010 may then extract Doppler components from the received echo signal to generate a Doppler signal. For example, the processor 1010 may perform quadrature demodulation on the received echo signal to acquire a complex baseband ultrasound signal as a Doppler signal. Thus, the processor 1010 may acquire a Doppler signal corresponding to the sample volume every period according to a PRF. Furthermore, the processor 1010 may acquire a Doppler signal corresponding to the sample volume repeatedly by an ensemble number.

[0072] According to another embodiment, the processor 1010 may acquire a Doppler signal corresponding to the sample volume from an external server or external device via the communication module 160 of the ultrasonic imaging apparatus 1000. According to another embodiment, the processor 1010 may acquire a prestored Doppler signal corresponding to the sample volume from the storage 150 of the ultrasonic imaging apparatus 1000.

[0073] The processor 1010 may divide an acquired Doppler signal into a plurality of sub-Doppler signals. According to an embodiment, the processor 1010 may divide a sample volume into a plurality of sections along a direction in which an ultrasound signal is transmitted and divide a Doppler signal into a plurality of sub-Doppler signals respectively corresponding to the plurality of sections. Furthermore, the processor 1010 may determine, based on a user input, the number and size of the plurality of sections set in the sample volume, and accordingly, determine the number and magnitude of the plurality of sub-Doppler signals.

[0074] Furthermore, the processor 1010 may divide each of a plurality of Doppler signals acquired every period according to a PRF into a plurality of sub-Doppler signals and repeatedly divide a Doppler signal into a plurality of sub-Doppler signals by an ensemble number.

[0075] The processor 1010 may generate a plurality of spectral Doppler signals by performing spectral analysis on each of a plurality of sub-Doppler signals. Spectral analysis refers to a process of estimating a Doppler signal in a time domain as a spectrum in a frequency domain, e. g., a process of converting a Doppler signal in the time domain into a spectral Doppler signal in the frequency domain. According to an embodiment, the spectral analysis may include performing weighting accumulation on a Doppler signal and performing fast Fourier transform (FFT) on the resulting signal. Thus, the processor 1010 may generate a plurality of spectral Doppler signals by performing weighting accumulation and FFT on the respective sub-Doppler signals.

[0076] The processor 1010 may generate a spectral Doppler signal corresponding to a sample volume from a plurality of spectral Doppler signals. According to an embodiment, the processor 1010 may generate a spectral Doppler signal corresponding to a sample volume by performing weighting accumulation on a plurality of spectral Doppler signals. According to another embodiment, the processor 1010 may determine at least one effective spectral Doppler signal from among a plurality of spectral Doppler signals and generate a spectral Doppler signal corresponding to a sample volume from the determined at least one spectral Doppler signal. For example, the processor 1010 may determine spectral Doppler signals representing an object from among a plurality of spectral Doppler signals and generate a spectral Doppler signal corresponding to a sample volume.

[0077] The display 1020 may display the generated spectral Doppler signal.

[0078] FIG. 4 is a diagram illustrating an embodiment in which the ultrasonic imaging apparatus 1000 generates a spectral Doppler signal corresponding to a sample volume.

[0079] According to an embodiment, the display 1020 may display a B-mode ultrasound image 401 showing an object. Subsequently, the processor 1010 may set a sample volume with respect to the object based on a user input. For example, the processor 1010 may set a sample volume with respect to a specific blood vessel.

[0080] The processor 1010 may acquire a Doppler signal 410 corresponding to the sample volume.

[0081] The processor 1010 may then divide the Doppler signal 410 into a plurality of sub-Doppler signals 412, 414, and 416. For example, the processor 1010 may divide the sample volume into first through N-th sections according to a direction in which an ultrasound signal is transmitted and divide the Doppler signal 410 into the plurality of sub-Doppler signals 412, 414, and 416 respectively corresponding to the first through N-th sections set in the sample volume.

[0082] Thereafter, the processor 1010 may generate a plurality of spectral Doppler signals by performing spectral analysis on each of the sub-Doppler signals 412, 414, and 416. In detail, the processor 1010 may generate first through N-th spectral Doppler signals by performing spectral analysis such as weighting accumulation and FFT on the sub-Doppler signals 412, 414, and 416.

[0083] The processor 1010 may then generate, from the plurality of spectral Doppler signals, a spectral Doppler signal corresponding to the sample volume. According to an embodiment, the processor 1010 may generate a spectral Doppler signal corresponding to the sample volume by performing weighting accumulation on the plurality of spectral Doppler signals.

[0084] FIG. 5 is a diagram illustrating a detailed embodiment in which an ultrasonic imaging apparatus generates a spectral Doppler signal corresponding to a sample volume.

[0085] The processor 1010 may divide a Doppler signal corresponding to a sample volume into a plurality of sub-Doppler signals and perform spectral analysis on each of the plurality of sub-Doppler signals.

[0086] First, the processor 1010 may perform weighting accumulation on each of the plurality of sub-Doppler signals. In detail, the processor 1010 may perform weighting accumulation on an m-th sub-Doppler signal from among a number of M sub-Doppler signals by using Equation (1) below:

$$c_m(t, 1) = \sum_{n=0}^N w(n) \cdot S_m(t + \Delta t, n) \quad \dots(1)$$

[0087] In Equation (1), $S_m(t + \Delta t, n)$ denotes a sub-Doppler signal $c_m(t, 1)$ (510) having a time interval of $\Delta t = 1/\text{PRF}$ and N pieces of sample data in a depth direction, $w(n)$ denotes a window function for weighting accumulation, and $c_m(t, 1)$ denotes a m-th sub-Doppler signal that has undergone the weighting accumulation. According to an embodiment, the window function $w(n)$ for weighting accumulation may be a hanning window function as shown in Equation (2). According to another embodiment, the window function $w(n)$ may be a trigometric window function, a Daniel window function, or a hamming window function.

$$w(n) = \begin{cases} \frac{1}{2} \left[1 - \cos\left(\frac{2\pi n}{N}\right) \right], & 0 \leq n \leq N \\ 0 & \end{cases} \quad \dots(2)$$

[0088] Subsequently, the processor 1010 may perform FFT on the Doppler signal c_m that has undergone the weighting accumulation by using Equation (3) below:

$$c_m(\omega) = \sum_{p=0}^{p-1} c_m e^{-jp\omega T} \quad \dots(3)$$

[0089] In Equation (3), the Doppler signal c_m that has undergone the weighting accumulation may denote P data sampled with a period $T = \Delta t$ in the time domain. Thus, the processor 1010 may perform weighting accumulation and FFT on each of the M sub-Doppler signals by using Equations (1) through (3).

[0090] Then, the processor 1010 may generate a spectral Doppler signal $X_m(t)$ by performing an absolute value (ABS) operation and log transformation on a Doppler signal $c_m(\omega)$ that has undergone Fourier transformation by using Equation (4) below:

$$X_m(t) = \log_{10}(|C_m(\omega)|) \quad \dots (4)$$

[0091] The processor 1010 may then generate a spectral Doppler signal $F(t)$ corresponding to a sample volume by performing weighting accumulation on a plurality of spectral Doppler signals X_1 through X_M by using Equation (5) below:

$$F(t) = \sum_{m=0}^M w_m \cdot X_m(t) \quad \dots (5)$$

[0092] According to an embodiment, in Equation (5), a window function w_m for weighting accumulation may be a hanning window function, a trigometric window function, a Daniel window function, a hamming window function, or the like.

[0093] FIG. 6 is a diagram illustrating an embodiment in which an ultrasonic imaging apparatus generates a spectral Doppler signal corresponding to a sample volume.

[0094] The processor 1010 may acquire a Doppler signal 610 corresponding to a sample volume set in an ultrasound image 601. The processor 1010 may then divide the Doppler signal 610 into sub-Doppler signals 612, 614, 616, and 618. Subsequently, the processor 1010 may generate spectral Doppler signals 622, 624, 626, and 628 by performing spectral analysis on each of the sub-Doppler signals 612, 614, 616, and 618. Although FIG. 6 shows four (4) sub-Doppler signals and four spectral Doppler signals, the number of sub-Doppler signals and the number of spectral Doppler signals are not limited thereto.

[0095] Then, the processor 1010 may then determine the spectral Doppler signals 624 and 626 to be effective from among the spectral Doppler signals 622, 624, 626, and 628. According to an embodiment, the processor 1010 may determine the spectral Doppler signals 624 and 626 containing relatively little artifact among the spectral Doppler signals 622, 624, 626, and 628 as effective spectral Doppler signals. According to another embodiment, when the sample volume is set with respect to a specific blood vessel, the processor 1010 may determine the spectral Doppler signals 624 and 626 representing the specific blood vessel from among the spectral Doppler signals 622, 624, 626, and 628 as effective spectral Doppler signals. Even though the sample volume is set with respect to a specific blood vessel, a section of the sample volume may not include the specific blood vessel when the blood vessel is small or a patient moves.

[0096] Next, the processor 1010 may generate a spectral Doppler signal 630 corresponding to the sample volume by using the effective spectral Doppler signals 624 and 626. According to an embodiment, the processor 1010 may generate the spectral Doppler signal 630 by performing weighting accumulation on the spectral Doppler signals 624 and 626 determined to be effective.

[0097] Thus, the ultrasonic imaging apparatus 1000 may divide a Doppler signal corresponding to a sample volume into a plurality of sub-Doppler signals and generate a spectral Doppler signal corresponding to the sample volume from a plurality of spectral Doppler signals respectively corresponding to the plurality of sub-Doppler signals. Thus, the special Doppler signal corresponding to the sample volume may be displayed as a high quality image. In other words, by displaying a spectral Doppler signal corresponding to the sample volume by partially performing weighting accumulation and Fourier transformation on the Doppler signal, the ultrasonic imaging apparatus 1000 is capable of displaying an image from which speckle noise is removed and with a clear boundary of a Doppler spectrum.

[0098] Furthermore, the ultrasonic imaging apparatus 1000 may generate a spectral Doppler signal corresponding to the sample volume by determining an effective spectral Doppler signal from among a plurality of spectral Doppler signals respectively corresponding to sections of the sample volume. Thus, the ultrasonic imaging apparatus 1000 may generate and display a more accurate spectral Doppler signal corresponding to the sample volume.

[0099] FIG. 7 is a flowchart of a method whereby an ultrasonic imaging apparatus displays an ultrasound image, according to an embodiment.

[0100] The method illustrated in FIG. 7 may be performed by each of the components of the ultrasonic imaging apparatus 1000 of FIG. 3, and repeated descriptions with respect to FIG. 3 will be omitted here.

[0101] In operation S710, the ultrasonic imaging apparatus 1000 may acquire a Doppler signal corresponding to a sample volume.

[0102] According to an embodiment, the ultrasonic imaging apparatus 1000 may control a probe to transmit, to a sample volume, an ultrasound signal which is generated according to a predetermined pulse repetition frequency (PRF) and receive an echo signal reflected from the sample volume. The ultrasonic imaging apparatus 1000 may then extract Doppler components with respect to the received echo signal to generate a Doppler signal.

[0103] According to another embodiment, the ultrasonic imaging apparatus 1000 may acquire a Doppler signal corresponding to a sample volume from an external server or an external device via a communication module. According to another embodiment, the ultrasonic imaging apparatus 1000 may acquire a Doppler signal corresponding to the sample volume prestored in a storage.

[0104] In operation S720, the ultrasonic imaging apparatus 1000 may divide the Doppler signal into a plurality of sub-Doppler signals. According to an embodiment, the ultrasonic imaging apparatus 1000 may divide the sample volume into a plurality of sections along a direction in which an ultrasound signal is transmitted and divide the Doppler signal into a plurality of sub-Doppler signals respectively corresponding to the plurality of sections. Furthermore, the ultrasonic imaging apparatus 1000 may determine, based on a user input, the number and size of the plurality of sections set in the sample volume, and accordingly, determine the number and magnitude of the plurality of sub-Doppler signals.

[0105] In operation S730, the ultrasonic imaging apparatus 1000 may generate a plurality of spectral Doppler signals by performing spectral analysis on each of the sub-Doppler signals. The ultrasonic imaging apparatus 1000 may generate a plurality of spectral Doppler signals by performing weighting accumulation and FFT with respect to the respective sub-Doppler signals.

[0106] In operation S740, the ultrasonic imaging apparatus 1000 may generate, from the plurality of spectral Doppler signals, a spectral Doppler signal corresponding to the sample volume.

[0107] According to an embodiment, the ultrasonic imaging apparatus 1000 may generate a spectral Doppler signal corresponding to the sample volume by performing weighting accumulation on the plurality of spectral Doppler signals. According to another embodiment, the ultrasonic imaging apparatus 1000 may determine at least one effective spectral Doppler signal from among the plurality of spectral Doppler signals and generate a spectral Doppler signal corresponding to the sample volume based on the determined at least one spectral Doppler signal.

[0108] In operation S750, the ultrasonic imaging apparatus 1000 may display the spectral Doppler signal corresponding to the sample volume.

[0109] FIG. 8 is a block diagram of an ultrasonic imaging apparatus 2000 according to another embodiment.

[0110] The ultrasonic imaging apparatus 2000 may include a processor 2010 and a display 2020. According to an embodiment, the processor 2010 may correspond to at least one or a combination of the image processor 130 and the controller 120 described with reference to FIG. 1, and the display 2020 may correspond to the display 140 of FIG. 1.

[0111] FIG. 8 shows that the ultrasonic imaging apparatus 2000 includes only components related to the present embodiment. Thus, it will be understood by those of ordinary skill in the relevant art that the ultrasonic imaging apparatus 2000 may include other common components as well as the components shown in FIG. 8. For example, the ultrasonic imaging apparatus 2000 may include at least one of the probe 20, the ultrasound transceiver 110, the storage 150, the communication module 160, and the input interface 170 described with reference to FIG. 1.

[0112] Furthermore, because the processor 2010 and the display 2020 may respectively correspond to the processor 1010 and the display 1020 described with reference to FIG. 3, repeated descriptions with respect to FIG. 3 will be omitted here.

[0113] The processor 2010 may acquire a Doppler signal corresponding to a sample volume.

[0114] The processor 2010 may divide an acquired Doppler signal into a plurality of sub-Doppler signals respectively corresponding to a plurality of sections set in the sample volume. In detail, the processor 2010 may segment the sample volume into a plurality of sections along a direction in which an ultrasound signal is transmitted or an axial direction of the sample volume and divide the Doppler signal into a plurality of sub-Doppler signals respectively corresponding to the plurality of sections. Furthermore, the processor 2010 may determine, based on a user input, the number and size of the plurality of sections set in the sample volume, and accordingly, determine the number and magnitude of the plurality of sub-Doppler signals.

[0115] The processor 2010 may generate a plurality of spectral Doppler signals by performing spectral analysis on

each of the plurality of sub-Doppler signals. According to an embodiment, the processor 2010 may generate a plurality of spectral Doppler signals by performing weighting accumulation and FFT on the respective sub-Doppler signals.

[0116] According to an embodiment, when the sample volume is set with respect to a blood vessel, the processor 2010 may provide blood flow characteristics in a plurality of sections set in the sample volume by using a plurality of spectral Doppler signals respectively corresponding to the plurality of sections. For example, for each of a plurality of sections, the processor 2010 may provide a user with changes in frequency and velocity of blood flow with respect to time, and may also calculate and provide to the user a peak velocity, a mean velocity, a peak gradient, an acceleration time, a deceleration time, a peak systolic velocity (PSV), an end diastolic velocity, a resistive index, a pulsatility index, etc.

[0117] The display 2020 may display the generated spectral Doppler signals.

[0118] Furthermore, according to an embodiment, the processor 2010 may generate a plurality of spectral lines respectively corresponding to the plurality of sections of the sample volume by respectively performing line tracing on the plurality of spectral Doppler signals, and the display 2020 may display the plurality of spectral lines. Line tracing is a technique for detecting a mean or peak velocity of a spectrum represented by a spectral Doppler signal and tracing a level of the detected mean or peak velocity.

[0119] FIG. 9 illustrates an embodiment in which the ultrasonic imaging apparatus 2000 displays a plurality of spectral Doppler signals.

[0120] According to an embodiment, the processor 2010 may acquire a Doppler signal 910 corresponding to a sample volume set in a B-mode ultrasound image 901. Furthermore, the processor 2010 may set a plurality of sections in the sample volume. In detail, the processor 2010 may set a plurality of sections along an axial direction on the sample volume. According to an embodiment, as shown in FIG. 9, the processor 2010 may divide the sample volume into first through N-th sections. For example, when the sample volume is set with respect to a blood vessel, the first section may be a section close to a blood vessel wall, and the N-th section may be a section close to an opposite blood vessel wall.

[0121] The processor 2010 may then divide the Doppler signal 910 into a plurality of sub-Doppler signals 912, 914, and 916 respectively corresponding to the plurality of sections set in the sample volume. In detail, the processor 2010 may divide the Doppler signal 910 into the sub-Doppler signals 912, 914, and 916 respectively corresponding to the first, second, and N-th sections of the sample volume.

[0122] Subsequently, the processor 2010 may generate a plurality of spectral Doppler signals respectively corresponding to the plurality of sections by performing spectral analysis on each of the sub-Doppler signals 912, 914, and 916. According to an embodiment, the processor 2010 may generate a plurality of spectral Doppler signals by performing weighting accumulation and FFT on the respective sub-Doppler signals 912, 914, and 916. For example, the processor 2010 may generate a plurality of spectral Doppler signals by applying Equations (1) through (4) of FIG. 5 to the respective sub-Doppler signals 912, 914, and 916. Thus, the processor 2010 may generate first, second, and N-th spectral Doppler signals respectively corresponding to the first, second, and N-th sections of the sample volume.

[0123] Then, the display 2020 may display the generated spectral Doppler signals.

[0124] Thus, the ultrasonic imaging apparatus 2000 may simultaneously display spectral Doppler signals respectively corresponding to a plurality of sections set in a sample volume, thereby providing information about the plurality of sections of the sample volume to the user. For example, when the sample volume is set with respect to a blood vessel, the ultrasonic imaging apparatus 2000 may simultaneously provide a user with various pieces of blood flow information regarding the plurality of sections in the blood vessel. Furthermore, the ultrasonic imaging apparatus may display spectral Doppler signals respectively corresponding to the sections of the sample volume based on a Doppler signal acquired every period according to a PRF, thereby providing information regarding each section of the sample volume during the same time.

[0125] FIG. 10 illustrates an embodiment in which the ultrasonic imaging apparatus 2000 displays a plurality of spectral Doppler signals as a single image.

[0126] According to an embodiment, the processor 2010 may overlap a plurality of spectral Doppler signals respectively corresponding to a plurality of sections set in a sample volume with one another. Then, the display 2020 may display the overlapped spectral Doppler signals as a single image.

[0127] Furthermore, according to an embodiment, the processor 2010 may generate a Doppler spectrum 1001 in which the overlapped spectral Doppler signals are respectively mapped in different colors. Then, the display 2020 may display the Doppler spectrum 1001. In other words, the display 2020 may respectively display spectral Doppler signals corresponding to first, second, and N-th sections of the sample volume in first, second, and N-th colors.

[0128] FIG. 11 illustrates an embodiment in which the ultrasonic imaging apparatus 2000 displays a plurality of spectral Doppler signals.

[0129] The processor 2010 may generate a plurality of spectral lines respectively corresponding to a plurality of sections set in a sample volume by respectively performing line tracing on a plurality of spectral Doppler signals. In detail, the processor 2010 may generate first, second, and N-th spectral lines respectively corresponding to first, second, and N-th spectral Doppler signals.

[0130] Thus, the processor 2010 may generate and control the display 2020 to display not only a plurality of spectral

Doppler signals representing the entire spectrum as shown in FIG. 9 but also spectral lines of the plurality of spectral Doppler signals as shown in FIG. 11.

[0131] FIG. 12 illustrates an embodiment in which the ultrasonic imaging apparatus 2000 provides information about vascular wall stiffness.

[0132] According to an embodiment, the processor 2010 may generate a single image by superimposing on one another spectral lines of a plurality of spectral Doppler signals respectively corresponding to a plurality of sections set in a sample volume.

[0133] Furthermore, the processor 2010 may detect a PSV in each of the plurality of sections of the sample volume based on the plurality of spectral Doppler signals or spectral lines. Furthermore, the processor 2010 may detect a difference between PSVs in the respective sections of the sample volume. For example, when the sample volume is set with respect to an artery, the processor 2010 may generate a spectral Doppler signal or a spectral line for each section of the artery. In other words, the processor 2010 may respectively generate spectral Doppler signals or spectral lines in a wall and a central section of the artery. Thus, the processor 2010 may detect a PSV in each section of the artery based on a spectral Doppler signal or a spectral line generated for each section of the artery and detect a difference between PSVs in the respective sections of the artery.

[0134] Referring to FIG. 12, when the sample volume is set with respect to a blood vessel, the processor 2010 may respectively generate spectra lines for sections of the blood vessel, and the display 2020 may display an image 1210 showing the generated spectra lines. Furthermore, the processor 2010 may detect a PSV in each of the sections of the blood vessel based on a spectral line corresponding to each section of the blood vessel. In addition, the processor 2010 may detect a difference APSV between maximum and minimum values selected from among PSVs detected in the respective sections of the blood vessel. For example, the difference Δ PSV may be a difference between PSVs in a section near a blood vessel wall and a central section of the blood vessel.

[0135] The processor 2010 may generate information about vascular wall stiffness based on a difference APSV. In the case of a blood vessel, a difference between blood flow velocities in each section of the blood vessel may vary according to vascular wall stiffness. For example, when the vascular wall stiffness increases, a difference between blood flow velocities in a central section and a wall of the blood vessel may decrease. When the vascular wall stiffness decreases, a difference between blood flow velocities in the central section and wall of the blood vessel may increase. Thus, the processor 2010 may detect a difference APSV for a patient's blood vessel and assess vascular wall stiffness in the patient based on the difference Δ PSV.

[0136] According to an embodiment, the processor 2010 may generate a graph 1220 as information about vascular wall stiffness. In detail, the processor 2010 may set a sample volume in a patient's blood vessel, generate a plurality of spectral Doppler signals respectively corresponding to a plurality of sections of the blood vessel, and detect a difference APSV for the blood vessel from the plurality of spectral Doppler signals. Furthermore, the processor 2010 may generate the graph 1220 for comparing detected difference Δ PSV for the patient with a prestored difference Δ PSV for a normal person. Thus, by displaying the graph 1220, the display 2020 may provide the patient with information representing comparison between vascular wall stiffness in the patient and vascular wall stiffness in the normal person.

[0137] FIG. 13 illustrates an embodiment in which the ultrasonic imaging apparatus 2000 displays a plurality of spectral Doppler signals.

[0138] The processor 2010 may set, based on a user input, a sample volume with respect to a blood vessel in a B-mode ultrasound image 1310. For example, the processor 2010 may set a sample volume with respect to a microscopic blood vessel in a kidney.

[0139] Next, the processor 2010 may acquire a Doppler signal corresponding to the sample volume and divide the acquired Doppler signal into first through tenth sub-Doppler signals respectively corresponding to first through tenth sections of the sample volume. The processor 2010 may then generate spectral Doppler signals respectively corresponding to the first through tenth sections of the sample volume by performing spectral analysis on each of the first through tenth sub-Doppler signals. As shown in FIG. 13, the display 2020 may display the spectral Doppler signals respectively corresponding to the first through tenth sections of the sample volume.

[0140] According to an embodiment, the ultrasonic imaging apparatus 2000 may include an input interface 170 via which a user may select at least one of spectral Doppler signals displayed on the display 2020. After selecting the at least one spectral Doppler signal, the display 2020 may display only the selected at least one spectral Doppler signal. For example, when the sample volume is set in a region including a microscopic blood vessel, it may be difficult to observe a spectral Doppler signal corresponding to the microscopic blood vessel due to movement such as human body's respiration. Thus, the ultrasonic imaging apparatus 2000 may provide the user with spectral Doppler signals respectively corresponding to the first through tenth sections, and the user may select, from among the provided spectral Doppler signals, spectral Doppler signals that respectively correspond to the sixth and seventh sections and best represent the microscopic blood vessel. Furthermore, according to an embodiment, the processor 2010 may perform weighting accumulation on the spectral Doppler signals, respectively corresponding to the sixth and seventh sections and being selected by the user, and display 2020 may display the spectral Doppler signals that have undergone the weighting

accumulation.

[0141] According to another embodiment, the processor 2010 may select at least one effective spectral Doppler signal from among the spectral Doppler signals respectively corresponding to the first through tenth sections. Then, the display 2020 may display the selected at least one effective spectral Doppler signal. For example, when the sample volume is set in a region including a blood vessel, the processor 2010 may select a spectral Doppler signal that best represents characteristics of the blood vessel from among the spectral Doppler signals respectively corresponding to the first through tenth sections. During this process, the processor 2010 may exclude, from the spectral Doppler signals, a spectral Doppler signal representing a spectrum of ultrasound signals reflected from a tissue or containing much artifact.

[0142] FIG. 14 illustrates a method whereby an ultrasonic imaging apparatus displays an ultrasound image, according to an embodiment.

[0143] The method illustrated in FIG. 14 may be performed by each of the components of the ultrasonic imaging apparatus 2000 of FIG. 8, and repeated descriptions with respect to FIG. 8 will be omitted here.

[0144] In operation S1410, the ultrasonic imaging apparatus 2000 may acquire a Doppler signal corresponding to a sample volume.

[0145] In operation S1420, the ultrasonic imaging apparatus 2000 may divide the Doppler signal into a plurality of sub-Doppler signals respectively corresponding to a plurality of sections set in the sample volume.

[0146] The ultrasonic imaging apparatus 2000 may divide the sample volume into a plurality of sections along a direction in which an ultrasound signal is transmitted or an axial direction of the sample volume and then divide the Doppler signal into a plurality of sub-Doppler signals respectively corresponding to the plurality of sections. Furthermore, the ultrasonic imaging apparatus 2000 may determine, based on a user input, the number and size of the plurality of sections set in the sample volume, and accordingly, determine the number and magnitude of the plurality of sub-Doppler signals.

[0147] In operation S1430, the ultrasonic imaging apparatus 2000 may generate a plurality of spectral Doppler signals respectively corresponding to the plurality of sections by performing spectral analysis on each of the sub-Doppler signals.

According to an embodiment, the ultrasonic imaging apparatus 2000 may generate a plurality of spectral Doppler signals by performing weighting accumulation and FFT on each of a plurality of sub-Doppler signals.

[0148] In operation S1440, the ultrasonic imaging apparatus 2000 may display the plurality of spectral Doppler signals.

[0149] Furthermore, the ultrasonic imaging apparatus 2000 may generate and display a plurality of spectral lines respectively corresponding to the plurality of sections of the sample volume by respectively performing line tracing on the plurality of spectral Doppler signals.

[0150] Furthermore, when the sample volume is set with respect to a blood vessel, the ultrasonic imaging apparatus 2000 may generate and display information about vascular wall stiffness based on the plurality of spectral Doppler signals.

[0151] In addition, when the sample volume is set with respect to an object, the ultrasonic imaging apparatus 2000 may select at least one spectral Doppler signal representing the object from among the plurality of spectral Doppler signals and display the selected at least one spectral Doppler signal.

[0152] FIG. 15 is a block diagram of an ultrasonic imaging apparatus 3000 according to another embodiment.

[0153] The ultrasonic imaging apparatus 3000 may include a processor 3010 and a display 3020. According to an embodiment, the processor 3010 may correspond to at least one or a combination of the image processor 130 and the controller 120 described with reference to FIG. 1, and the display 3020 may correspond to the display 140 of FIG. 1.

[0154] FIG. 15 shows that the ultrasonic imaging apparatus 3000 includes only components related to the present embodiment. Thus, it will be understood by those of ordinary skill in the relevant art that the ultrasonic imaging apparatus 3000 may include other common components as well as the components shown in FIG. 15. For example, the ultrasonic imaging apparatus 3000 may include at least one of the probe 20, the ultrasound transceiver 110, the storage 150, the communication module 160, and the input interface 170 described with reference to FIG. 1.

[0155] Furthermore, because the processor 3010 may correspond to the processors 1010 and 2010 respectively described with reference to FIGS. 3 and 8, and the display 3020 may correspond to the displays 1020 and 2020 respectively described with reference to FIGS. 3 and 8, descriptions that are already provided above with respect to FIGS. 3 and 8 will be omitted here.

[0156] The processor 3010 may acquire a Doppler signal corresponding to a sample volume that is set with respect to an object. The sample volume may be set with respect to a region including the object. For example, the sample volume may be set with respect to a region including a specific blood vessel. Furthermore, the processor 3010 may set a plurality of sections in the sample volume. In detail, the processor 3010 may set a plurality of sections in the sample volume along an axial direction on the sample volume.

[0157] The processor 3010 may generate a plurality of spectral Doppler signals respectively corresponding to the plurality of sections by performing spectral analysis on each of the Doppler signal in the plurality of sections. According to an embodiment, the processor 3010 may divide the Doppler signal into a plurality of sub-Doppler signals respectively corresponding to the plurality of sections set in the sample volume and perform a plurality of spectral analyses on the sub-Doppler signals to generate a plurality of spectral Doppler signals respectively corresponding to the plurality of

sections. According to an embodiment, the processor 3010 may generate a plurality of spectral Doppler signals by performing weighting accumulation and FFT on the respective sub-Doppler signals. For example, the processor 3010 may generate a plurality of spectral Doppler signals by applying Equations (1) through (4) of FIG. 5 to the respective sub-Doppler signals.

[0158] The processor 3010 may model an artifact signal in a spectral Doppler signal corresponding to an object by using a plurality of spectral Doppler signals.

[0159] First, the processor 3010 may determine a spectral Doppler signal corresponding to an object from among a plurality of spectral Doppler signals. In detail, according to an embodiment, the processor 3010 may determine a spectral Doppler signal corresponding to a section including an object from among a plurality of sections in a sample volume as a spectral Doppler signal corresponding to the object. According to another embodiment, the processor 3010 may generate a spectral Doppler signal corresponding to an object by performing weighting summation on spectral Doppler signals corresponding to two or more sections including the object from among a plurality of sections of a sample volume.

[0160] Next, the processor 3010 may determine an artifact signal in the spectral Doppler signal corresponding to the object. In detail, the spectral Doppler signal corresponding to the object may include not only a signal representing the object but also an ultrasound reflected signal from another object. In other words, the spectral Doppler signal corresponding to the object may be a signal in which a signal representing the object is superimposed with an ultrasound reflected signal from another object. For example, when an object is a specific blood vessel, a spectral Doppler signal corresponding to the object may be a signal where a signal representing the specific blood vessel is superimposed with an ultrasound reflected signal from another blood vessel or a particular tissue. Thus, the processor 3010 may determine as an artifact signal an ultrasound reflected signal from another object, which is contained in the spectral Doppler signal corresponding to the object.

[0161] The processor 3010 may then model the artifact signal. According to an embodiment, the processor 3010 may model the artifact signal by using a spectral Doppler signal corresponding to a section including another object from among the plurality of spectral Doppler signals. For example, when a spectral Doppler signal corresponding to one section including another object is included among the plurality of spectral Doppler signals, the processor 3010 may determine the spectral Doppler signal corresponding to the section including the other object as an artifact signal. As another example, when spectral Doppler signals respectively corresponding to two or more sections including another object are included among the plurality of spectral Doppler signals, the processor 3010 may generate an artifact signal by performing weighting summation on the spectral Doppler signals corresponding to the sections including the other object.

[0162] Based on the spectral Doppler signal corresponding to the object and the artifact signal, the processor 3010 may generate a spectral Doppler signal corresponding to the object and from which an artifact is removed. According to an embodiment, the processor 3010 may generate a spectral Doppler signal corresponding to the object and from which an artifact is removed by performing subtraction between the spectral Doppler signal corresponding to the object and the artifact signal. In other words, the processor 3010 may remove a signal representing another object from the spectral Doppler signal corresponding to the object by subtracting the artifact signal from the spectral Doppler signal corresponding to the object.

[0163] The display 3020 may display the spectral Doppler signal corresponding to the object and from which the artifact is removed.

[0164] FIG. 16 illustrates an embodiment in which the ultrasonic imaging apparatus 3000 generates a spectral Doppler signal corresponding to an object.

[0165] The processor 3010 may acquire a Doppler signal 1610 corresponding to a sample volume set in a B-mode ultrasound image 1601. Furthermore, the processor 3010 may set a plurality of sections in the sample volume.

[0166] The processor 3010 may then divide the Doppler signal 1610 into a plurality of sub-Doppler signals 1612, 1614, and 1616 respectively corresponding to the plurality of sections set in the sample volume.

[0167] The processor 3010 may generate a plurality of spectral Doppler signals respectively corresponding to the plurality of sections by performing spectral analysis on each of the sub-Doppler signals 1612, 1614, and 1616.

[0168] The processor 3010 may model an artifact signal in a spectral Doppler signal corresponding to an object by using the plurality of spectral Doppler signals.

[0169] First, the processor 3010 may determine a spectral Doppler signal corresponding to a section including an object from among the plurality of sections of the sample volume as a spectral Doppler signal corresponding to the object.

[0170] Next, the processor 3010 may determine an artifact signal in the spectral Doppler signal corresponding to the object. The processor 3010 may determine as an artifact signal an ultrasound reflected signal from another object, which is contained in the spectral Doppler signal corresponding to the object.

[0171] The processor 3010 may then determine a spectral Doppler signal corresponding to a section including another object as an artifact signal.

[0172] The processor 3010 may generate, based on the spectral Doppler signal corresponding to the object and the artifact signal, a spectral Doppler signal corresponding to the object and from which an artifact is removed.

[0173] FIG. 17 illustrates a detailed embodiment in which the ultrasonic imaging apparatus 3000 generates a spectral Doppler signal corresponding to an object.

[0174] The processor 3010 may acquire a Doppler signal 1710 corresponding to a sample volume set in an ultrasound image 1701. The sample volume may be set to include a venous region 1703 and an arterial region 1705.

[0175] The processor 3010 may divide the Doppler signal 1710 into a plurality of sub-Doppler signals 1712, 1714, and 1716 respectively corresponding to a plurality of sections set in the sample volume. The processor 3010 may then generate a plurality of spectral Doppler signals respectively corresponding to the plurality of sections by performing spectral analysis on each of the sub-Doppler signals 1712, 1714, and 1716.

[0176] The processor 3010 may determine a spectral Doppler signal corresponding to a section including a vein from among the plurality of sections of the sample volume as a spectral Doppler signal 1720 corresponding to an object. The spectral Doppler signal 1720 corresponding to the object may be a signal in which a spectral Doppler signal representing the vein is superimposed with an ultrasound reflected signal from an artery. Thus, the processor 3010 may determine the ultrasound reflected signal from the artery as an artifact signal in the spectral Doppler signal 1720 corresponding to the object.

[0177] The processor 3010 may determine as an artifact signal 1730 a spectral Doppler signal corresponding to a section including the artery from among the plurality of spectral Doppler signals.

[0178] The processor 3010 may generate, based on the spectral Doppler signal 1720 corresponding to the object and the artifact signal 1730, a spectral Doppler signal 1740 corresponding to the object and from which an artifact is removed. In other words, the processor 3010 may generate the spectral Doppler signal 1740 as a signal obtained by removing the ultrasound reflected signal from the artery from the spectral Doppler signal 1720.

[0179] According to another embodiment, unlike in FIG. 17, the processor 3010 may determine a spectral Doppler signal corresponding to a section including an artery from among the plurality of sections of the sample volume as a spectral Doppler signal corresponding to an object, and a spectral Doppler signal corresponding to a section including a vein from among the plurality of spectral Doppler signals as an artifact signal. In other words, because the spectral Doppler signal corresponding to the object may include not only a spectral Doppler signal representing the artery but also an ultrasound reflected signal from the vein, the spectral Doppler signal corresponding to the section including the vein may be determined as an artifact signal. Thus, the processor 3010 may generate a spectral Doppler signal as a signal obtained by removing the ultrasound reflected signal from the vein from the spectral Doppler signal corresponding to the artery.

[0180] FIG. 18 illustrates another embodiment in which the ultrasonic imaging apparatus 3000 generates a spectral Doppler signal corresponding to an object.

[0181] The ultrasonic imaging apparatus 3000 may include the ultrasound transceiver 110.

[0182] The ultrasound transceiver 110 may transmit ultrasound signals along a pulse Doppler line 1801 passing through a sample volume set with respect to an object and receive echo signals reflected from the sample volume and at least one volume on the pulse Doppler line 1801. The processor 3010 may acquire from the received echo signals a Doppler signal 1810 corresponding to the sample volume and at least one Doppler signal 1820 corresponding to the at least one volume.

[0183] The processor 3010 may generate a spectral Doppler signal corresponding to the object by performing spectral analysis on the Doppler signal 1810 corresponding to the sample volume. Furthermore, the processor 3010 may generate at least one spectral Doppler signal corresponding to the at least one volume by performing spectral analysis on the at least one Doppler signal 1820 corresponding to the at least one volume.

[0184] The processor 3010 may model an artifact signal in the spectral Doppler signal corresponding to the object by using the at least one spectral Doppler signal. The processor 3010 may determine as an artifact signal an ultrasound reflected signal from another object, which is contained in the spectral Doppler signal corresponding to the object. The processor 3010 may determine as an artifact signal a spectral Doppler signal corresponding to a volume including another object from among the at least one volume.

[0185] Thus, the processor 3010 may generate, based on the spectral Doppler signal corresponding to the object and the artifact signal, a spectral Doppler signal corresponding to the object and from which an artifact is removed.

[0186] FIG. 19 is a flowchart of a method whereby an ultrasonic imaging apparatus displays an ultrasound image, according to an embodiment.

[0187] The method illustrated in FIG. 19 may be performed by each of the components of the ultrasonic imaging apparatus 3000 of FIG. 15, and repeated descriptions with respect to FIG. 15 will be omitted here.

[0188] In operation S1910, the ultrasonic imaging apparatus 3000 may acquire a Doppler signal corresponding to a sample volume set with respect to an object. Furthermore, the ultrasonic imaging apparatus may set a plurality of sections in the sample volume.

[0189] In operation S1920, the ultrasonic imaging apparatus 3000 may generate a plurality of spectral Doppler signals respectively corresponding to the plurality of sections set in the sample volume by performing a spectral on each of the Doppler signal from the plurality of sections. According to an embodiment, the ultrasonic imaging apparatus 3000 may

divide the Doppler signal into a plurality of sub-Doppler signals respectively corresponding to the plurality of sections set in the sample volume and generate a plurality of spectral Doppler signals respectively corresponding to the plurality of sections by performing a plurality of spectral analyses. According to an embodiment, the ultrasonic imaging apparatus 300 may generate a plurality of spectral Doppler signals by performing weighting accumulation and FFT on the respective sub-Doppler signals.

[0190] In operation S1930, the ultrasonic imaging apparatus 3000 may model an artifact signal in a spectral Doppler signal corresponding to the object by using the plurality of spectral Doppler signals.

[0191] The ultrasonic imaging apparatus 3000 may determine a spectral Doppler signal corresponding to the object from among the plurality of spectral Doppler signals. The ultrasonic imaging apparatus 3000 may determine a spectral Doppler signal corresponding to a section including the object from among the plurality of sections of the sample volume as a spectral Doppler signal corresponding to the object.

[0192] The ultrasonic imaging apparatus 3000 may determine an artifact signal in the spectral Doppler signal corresponding to the object. The ultrasonic imaging apparatus 3000 may determine as an artifact signal an ultrasound reflected signal from another object, which is contained in the spectral Doppler signal corresponding to the object. The ultrasonic imaging apparatus 3000 may model an artifact signal by using a spectral Doppler signal corresponding to a section including another object from among the plurality of spectral Doppler signals.

[0193] In operation S1940, the ultrasonic imaging apparatus 3000 may generate, based on the spectral Doppler signal corresponding to the object and the artifact signal, a spectral Doppler signal corresponding to the object and from which an artifact is removed. The ultrasonic imaging apparatus 3000 may generate a spectral Doppler signal corresponding to the object and from which an artifact is removed by performing subtraction between the spectral Doppler signal corresponding to the object and the artifact signal.

[0194] In operation S1950, the ultrasonic imaging apparatus 3000 may display the spectral Doppler signal corresponding to the object and from which the artifact is removed.

[0195] The embodiments may be implemented through computer-readable recording media having stored thereon computer-executable instructions and data. The instructions may be stored in the form of program codes, and when executed by a processor, may generate a predetermined program module to perform a specific operation. Furthermore, when being executed by the processor, the instructions may perform specific operations according to the embodiments.

[0196] While embodiments of the disclosure have been particularly shown and described with reference to the accompanying drawings, it will be understood by those of ordinary skill in the art that various changes in form and details may be made therein without departing from the spirit and essential characteristics of the present disclosure. Accordingly, the above embodiments and all aspects thereof are examples only and are not limiting.

Claims

1. An ultrasonic imaging apparatus comprising:

a processor configured to acquire a Doppler signal corresponding to a sample volume, divide the Doppler signal into a plurality of sub-Doppler signals, generate a plurality of spectral Doppler signals by performing spectral analysis on each of the plurality of sub-Doppler signals, and generate, from the plurality of spectral Doppler signals, a spectral Doppler signal corresponding to the sample volume; and
a display displaying the spectral Doppler signal corresponding to the sample volume.

2. The ultrasonic imaging apparatus of claim 1, wherein the processor is further configured to generate the plurality of spectral Doppler signals by performing weighting accumulation and Fourier Transform on each of the plurality of sub-Doppler signals.

3. The ultrasonic imaging apparatus of claim 1, wherein the processor is further configured to generate the spectral Doppler signal corresponding to the sample volume by performing weighting accumulation on the plurality of spectral Doppler signals.

4. The ultrasonic imaging apparatus of claim 1, wherein the processor is further configured to divide the Doppler signal into the plurality of sub-Doppler signals respectively corresponding to a plurality of sections set in the sample volume.

5. The ultrasonic imaging apparatus of claim 4, wherein the processor is further configured to generate the plurality of spectral Doppler signals respectively corresponding to the plurality of sections, and wherein the display displays the plurality of spectral Doppler signals.

6. The ultrasonic imaging apparatus of claim 4, wherein the number and length of the plurality of sections are set based on a user input.

7. The ultrasonic imaging apparatus of claim 1, wherein the processor is further configured to:

determine at least one effective spectral Doppler signal from among the plurality of spectral Doppler signals; and generate the spectral Doppler signal corresponding to the sample volume from the determined at least one spectral Doppler signal.

8. The ultrasonic imaging apparatus of claim 1, further comprising an ultrasound transceiver configured to control a probe to transmit a generated ultrasound signal to the sample volume as many times as a predetermined ensemble number and according to a preset pulse repetition frequency (PRF), and receive an echo signal reflected from the sample volume, wherein the processor is further configured to acquire the Doppler signal based on the echo signal.

9. The ultrasonic imaging apparatus of claim 1, wherein the processor is further configured to acquire the Doppler signal corresponding to the sample volume set with respect to an object, model an artifact signal in a spectral Doppler signal corresponding to the object by using the plurality of spectral Doppler signals, and generate, based on the spectral Doppler signal corresponding to the object and the artifact signal, a spectral Doppler signal corresponding to the object and from which an artifact is removed, and wherein the display displays the spectral Doppler signal corresponding to the object and from which the artifact is removed.

10. A method of displaying an ultrasound image, the method comprising:

acquiring a Doppler signal corresponding to a sample volume;
dividing the Doppler signal into a plurality of sub-Doppler signals;
generating a plurality of spectral Doppler signals by performing spectral analysis on each of the plurality of sub-Doppler signals;
generating, from the plurality of spectral Doppler signals, a spectral Doppler signal corresponding to the sample volume; and
displaying the spectral Doppler signal corresponding to the sample volume.

11. The method of claim 10, wherein the generating of the plurality of spectral Doppler signals comprises generating the plurality of spectral Doppler signals by performing weighting accumulation and Fourier Transform on each of the plurality of sub-Doppler signals.

12. The method of claim 10, wherein the generating of the spectral Doppler signal corresponding to the sample volume comprises generating the spectral Doppler signal corresponding to the sample volume by performing weighting accumulation on the plurality of spectral Doppler signals, and wherein the dividing of the Doppler signal comprises dividing the Doppler signal into the plurality of sub-Doppler signals respectively corresponding to a plurality of sections set in the sample volume.

13. The method of claim 10, further comprising:

determining at least one effective spectral Doppler signal from among the plurality of spectral Doppler signals; and generating the spectral Doppler signal corresponding to the sample volume from the determined at least one spectral Doppler signal.

14. The method of claim 10, further comprising controlling a probe to transmit a generated ultrasound signal to the sample volume by as many times as a predetermined ensemble number and according to a preset pulse repetition frequency (PRF), and receiving an echo signal reflected from the sample volume, wherein the acquiring of the Doppler signal comprises acquiring the Doppler signal based on the echo signal.

15. A computer-readable recording medium having recorded thereon a program for executing the method of claim 10 on a computer.

FIG. 1

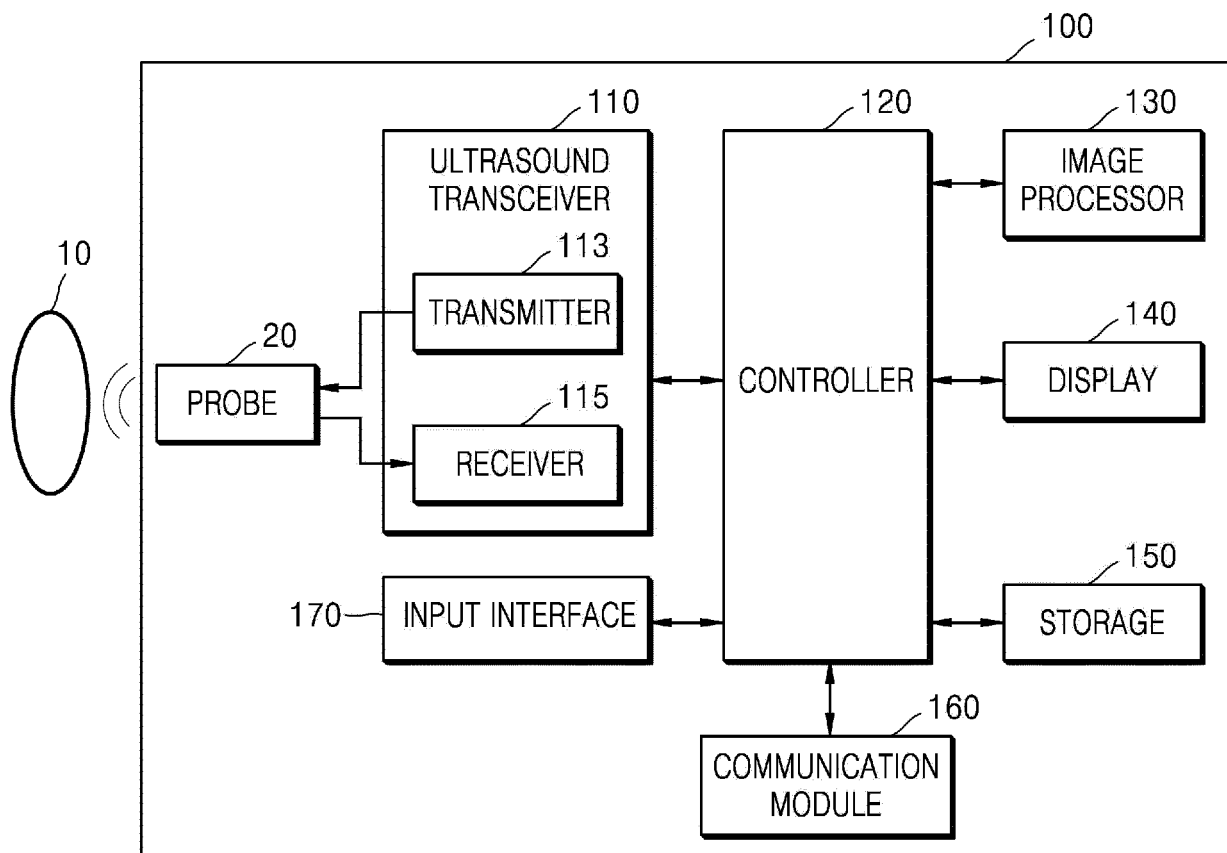


FIG. 2C

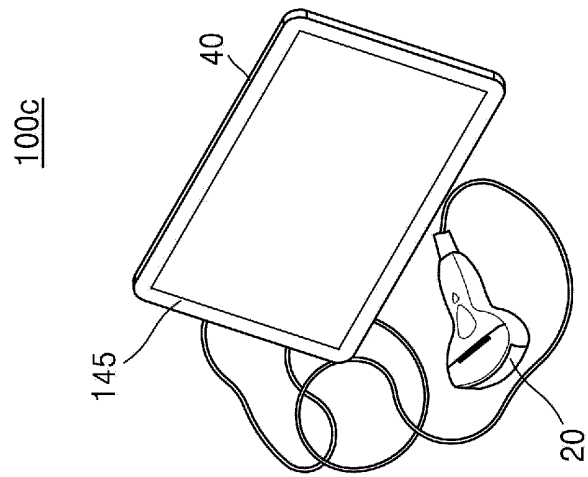


FIG. 2B

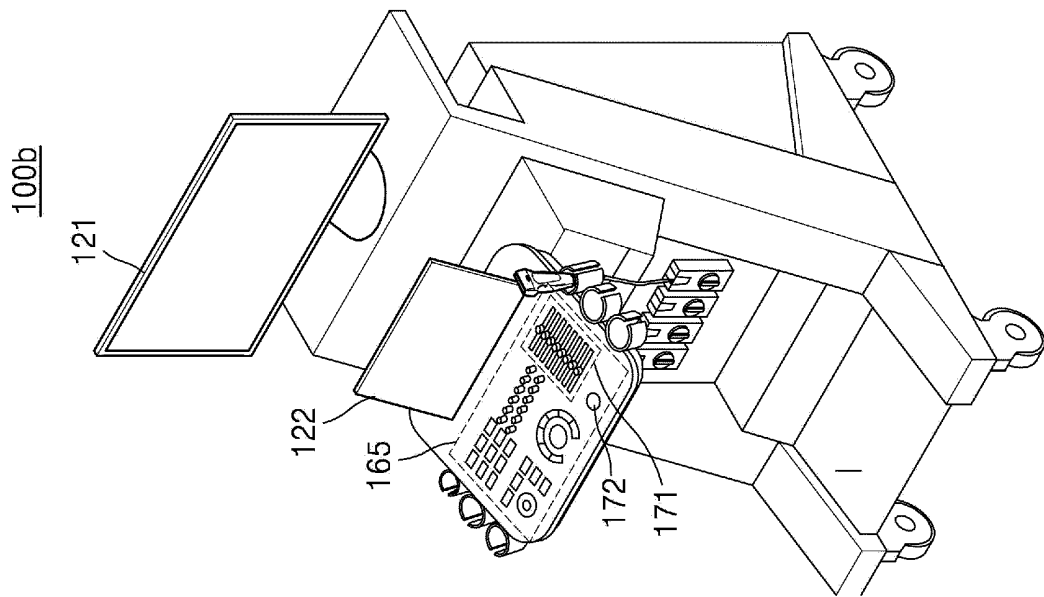


FIG. 2A

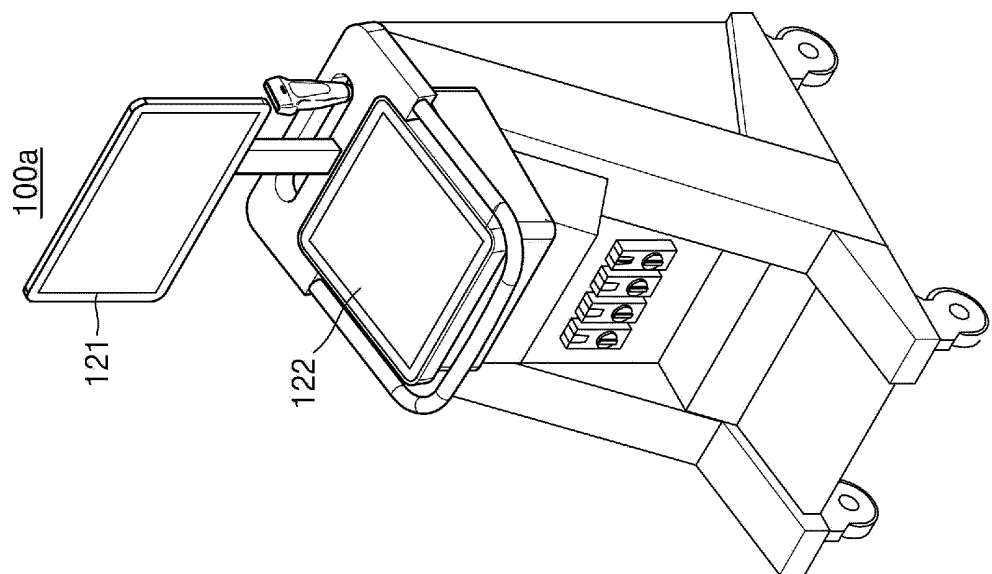


FIG. 3

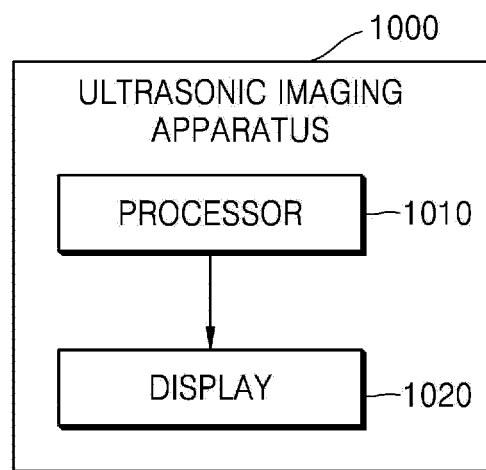


FIG. 4

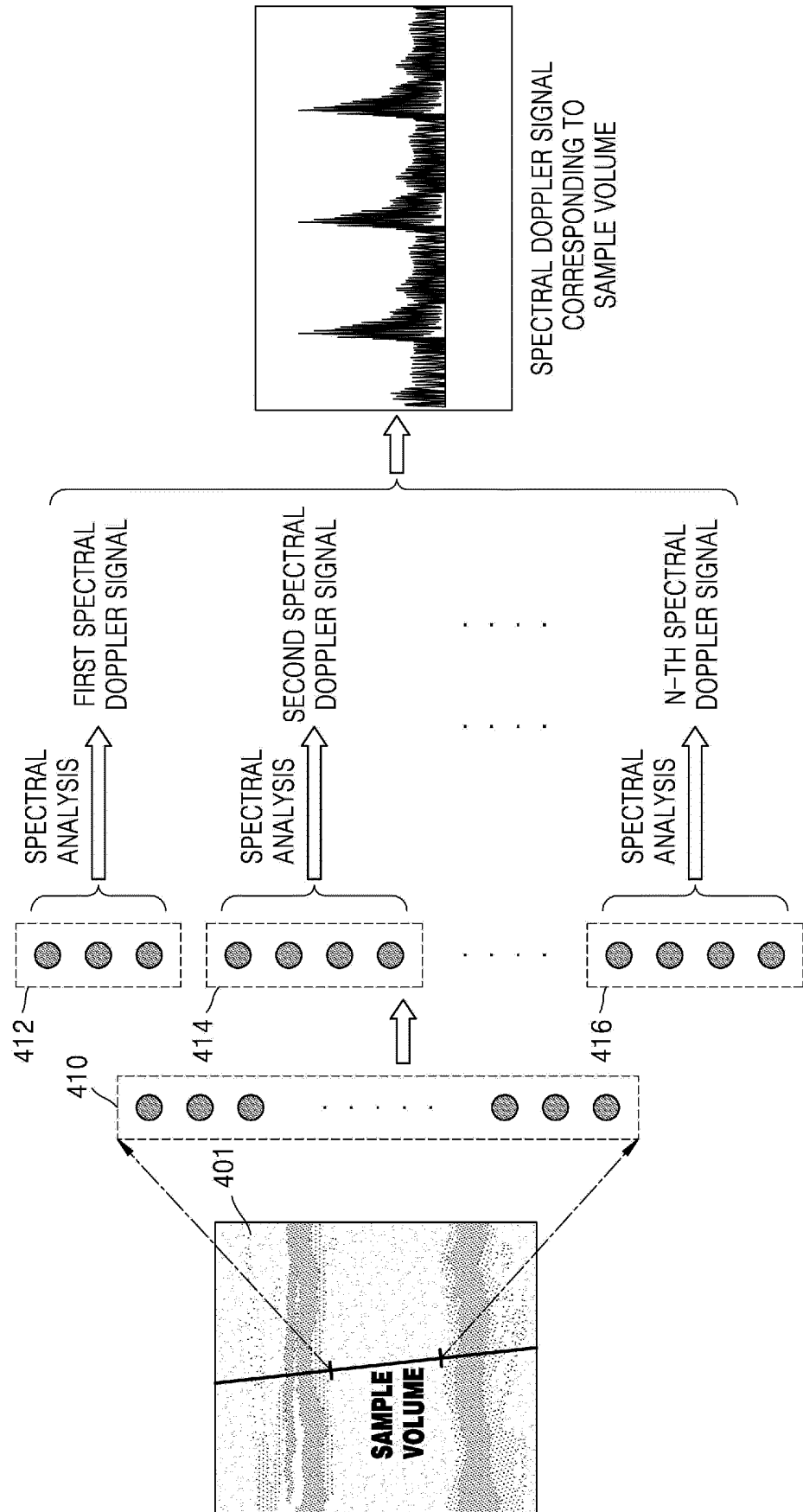


FIG. 5

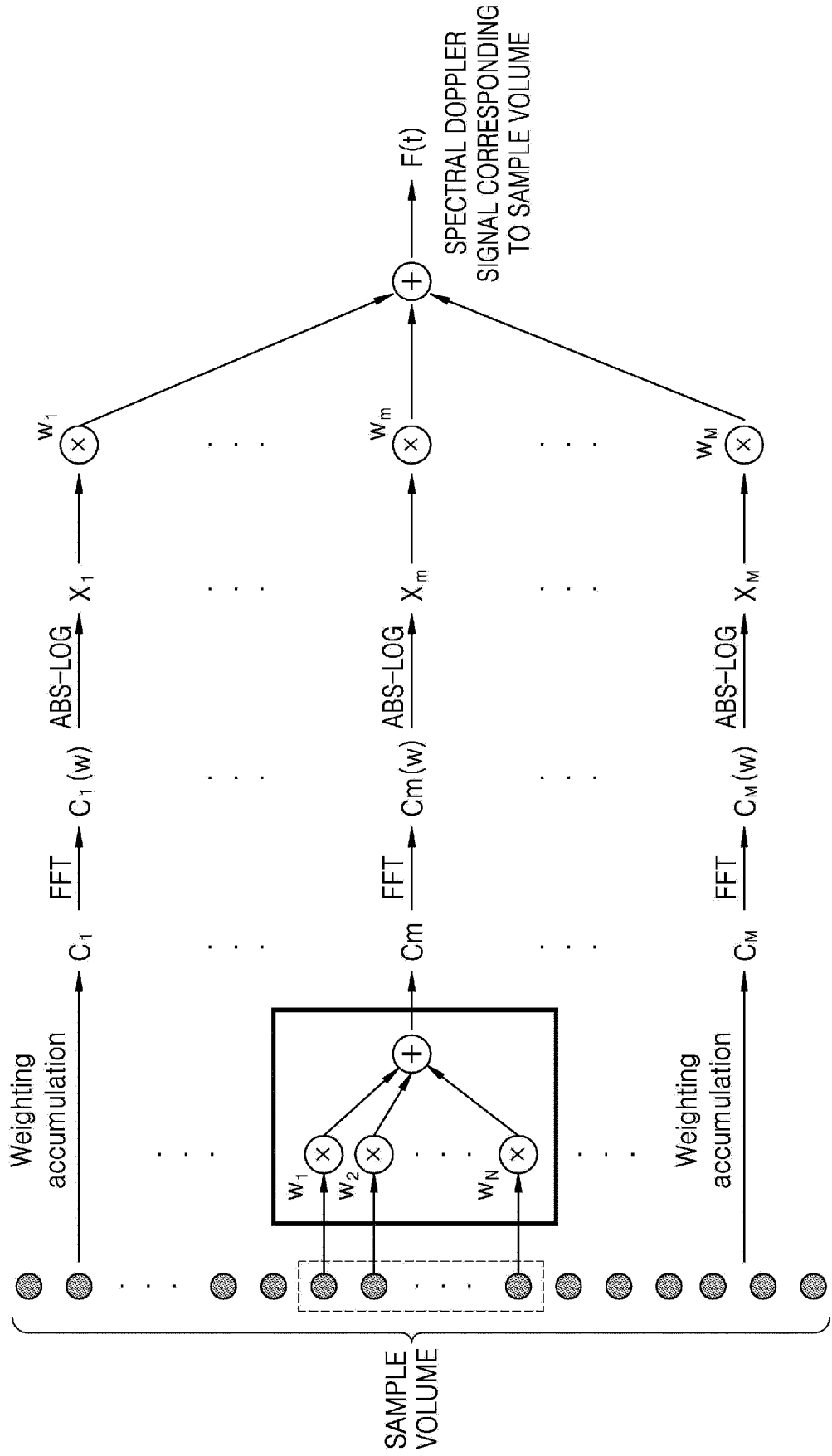


FIG. 6

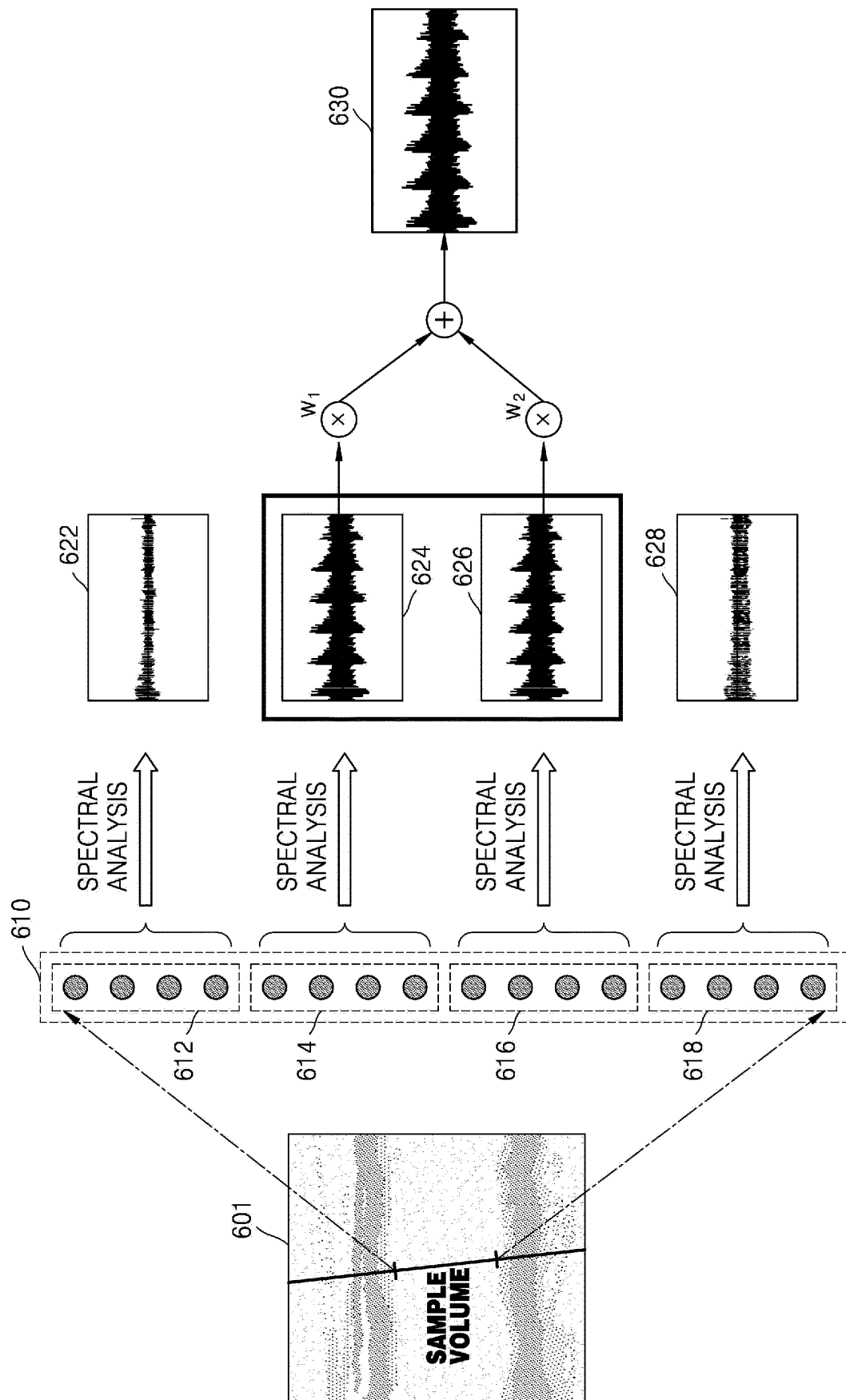


FIG. 7

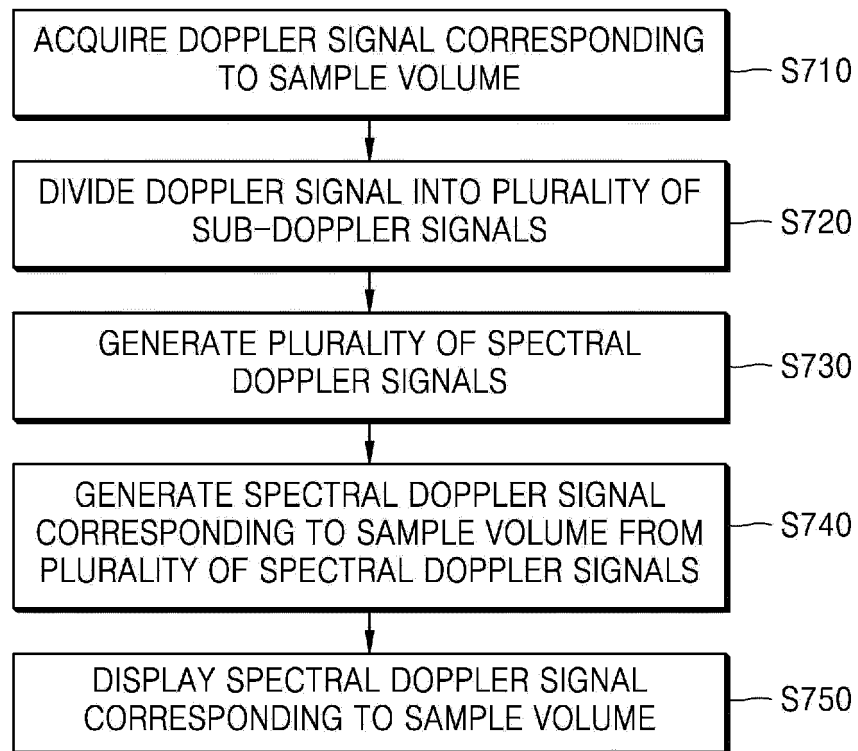


FIG. 8

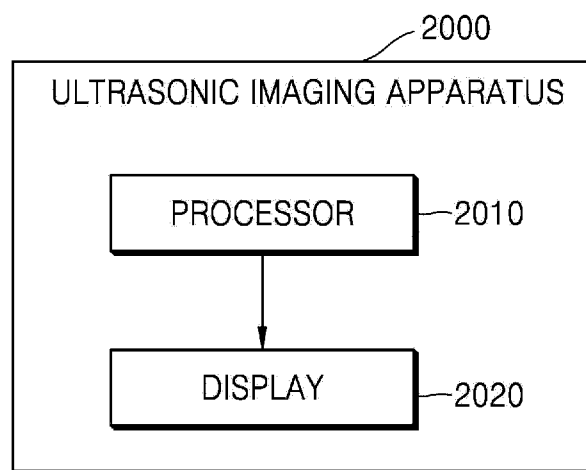


FIG. 9

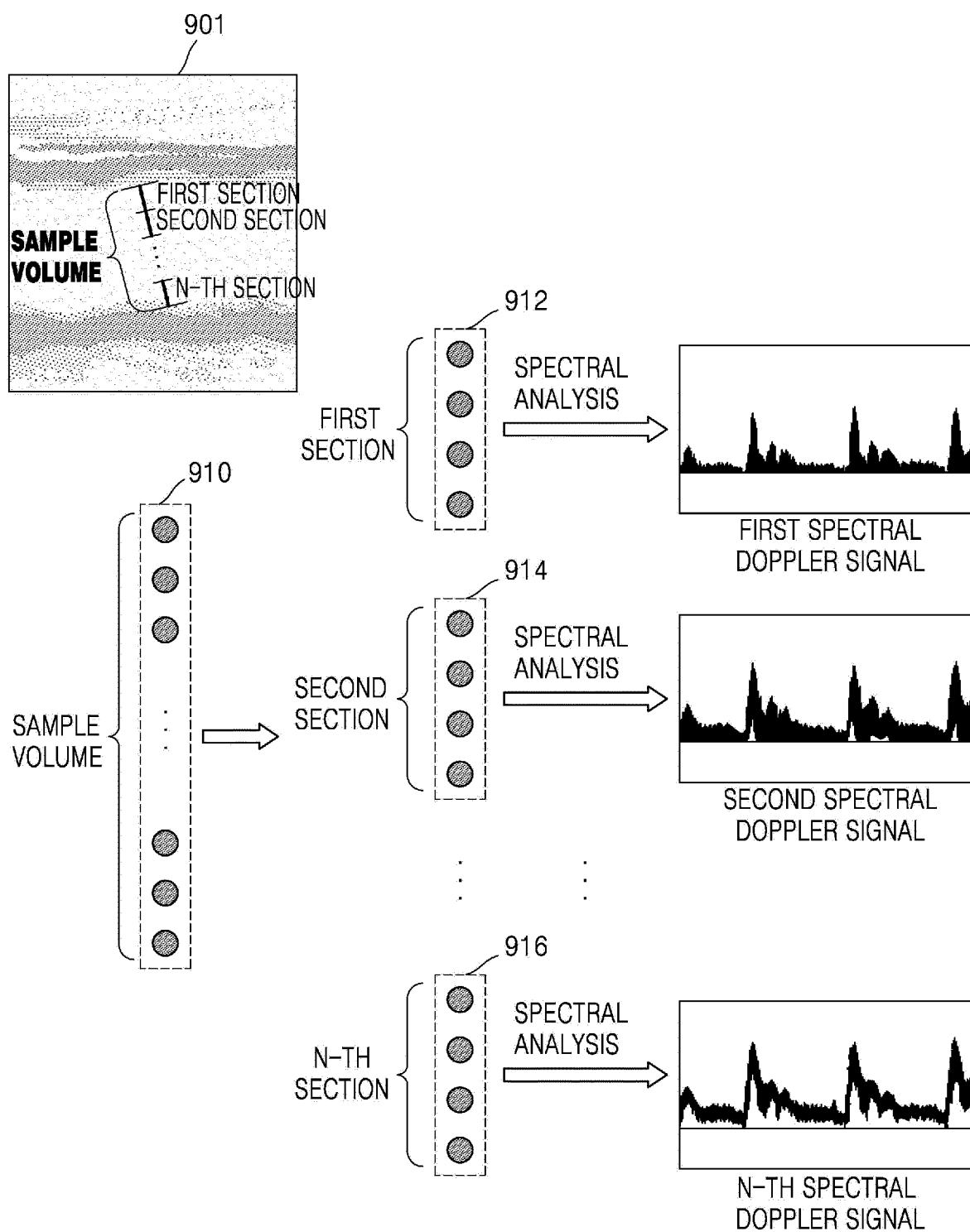


FIG. 10

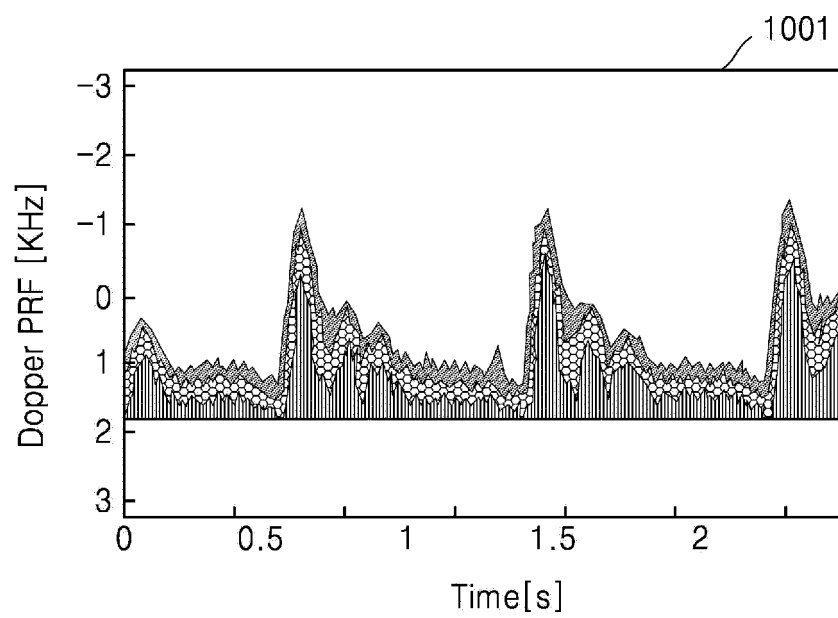


FIG. 11

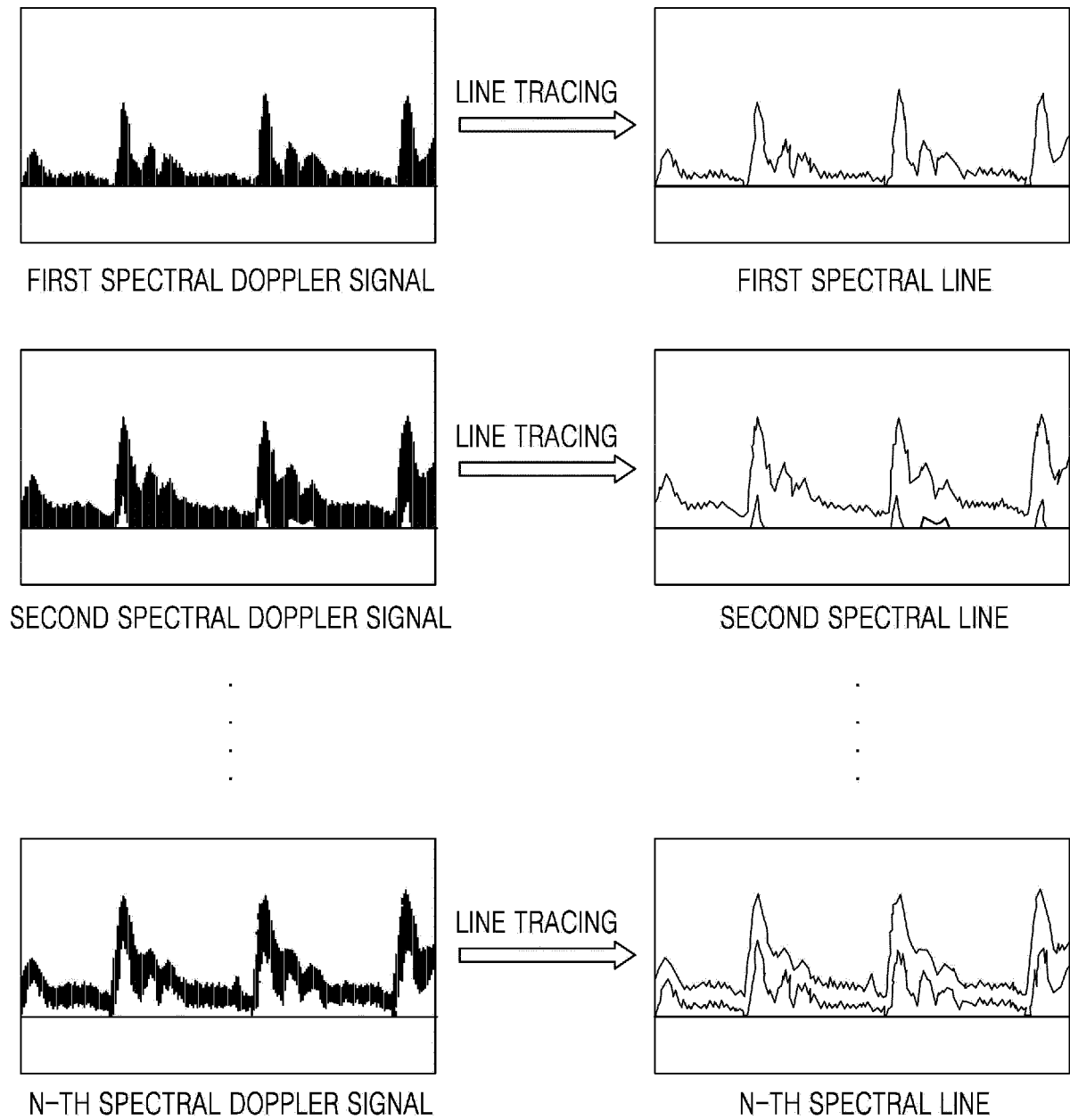


FIG. 12

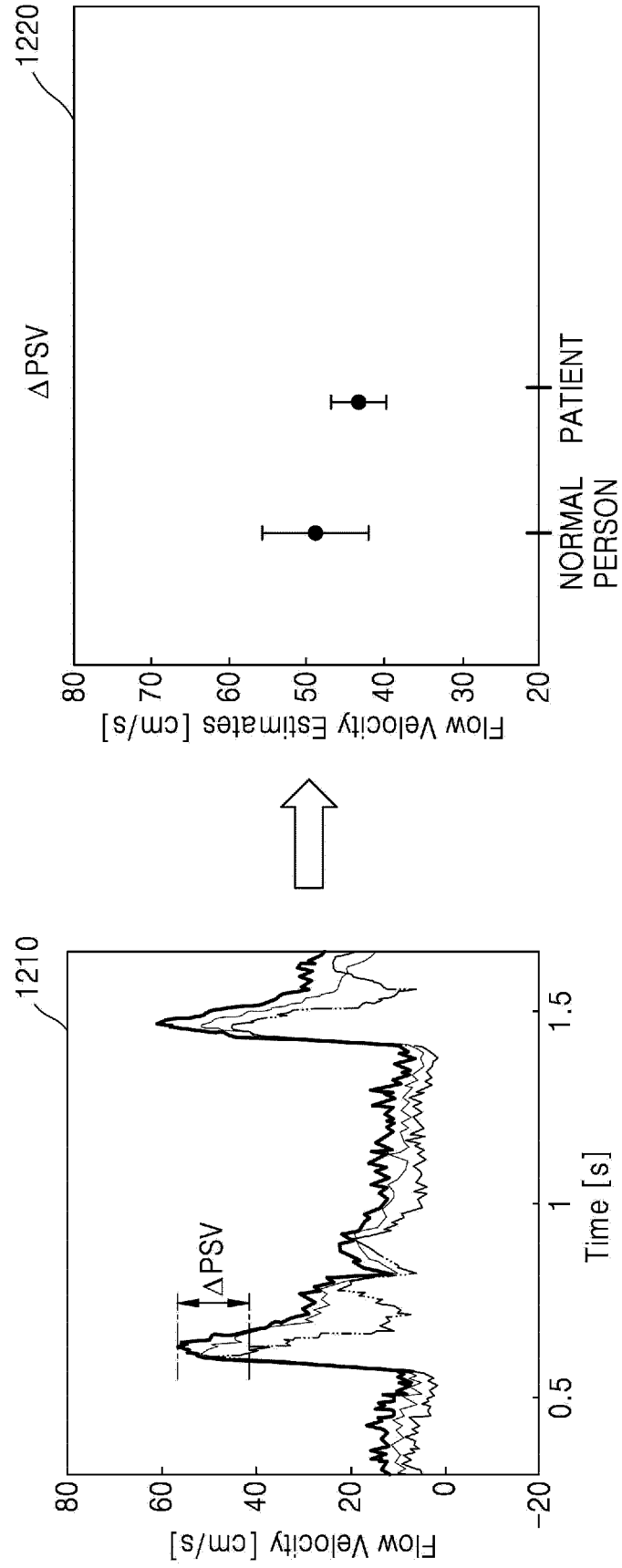


FIG. 13

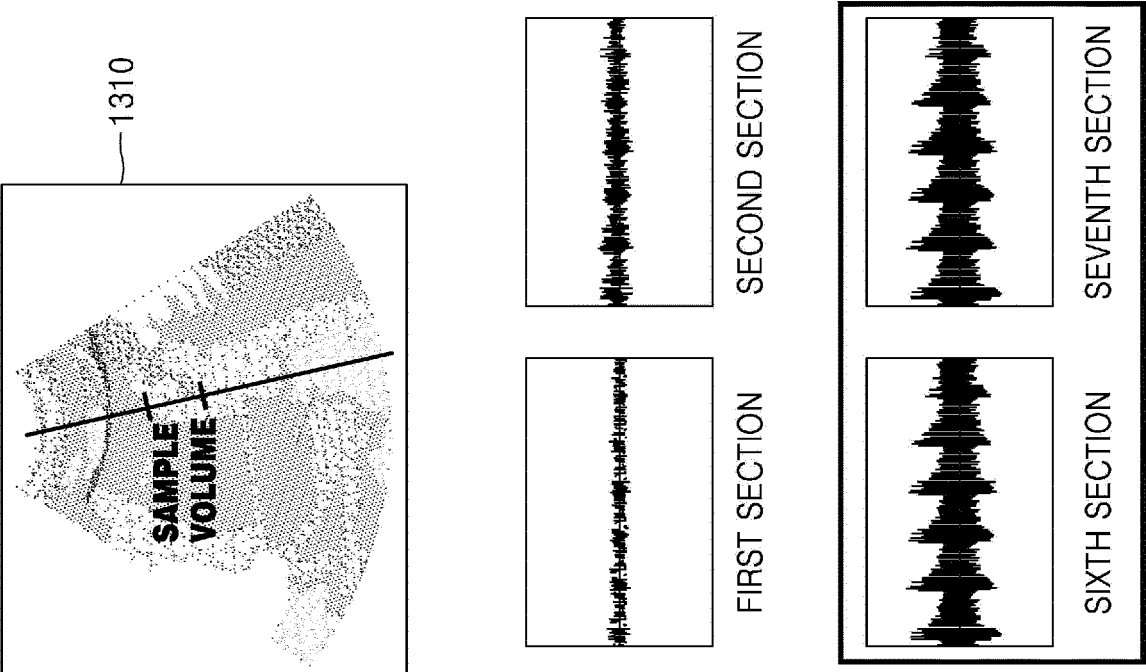


FIG. 14

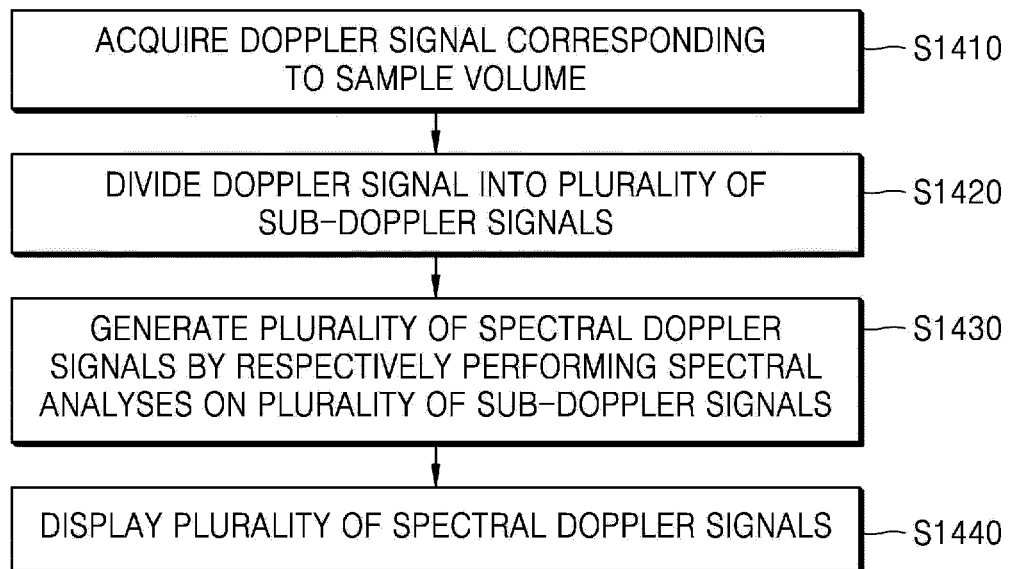
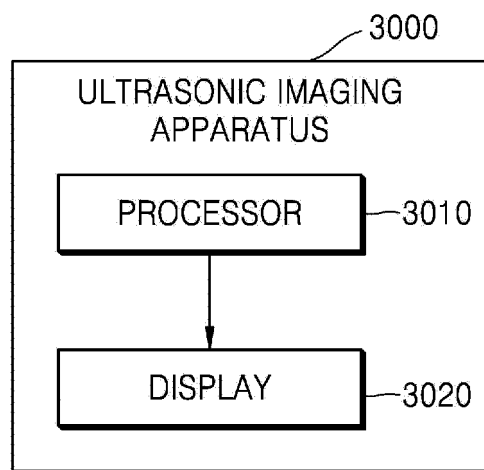


FIG. 15



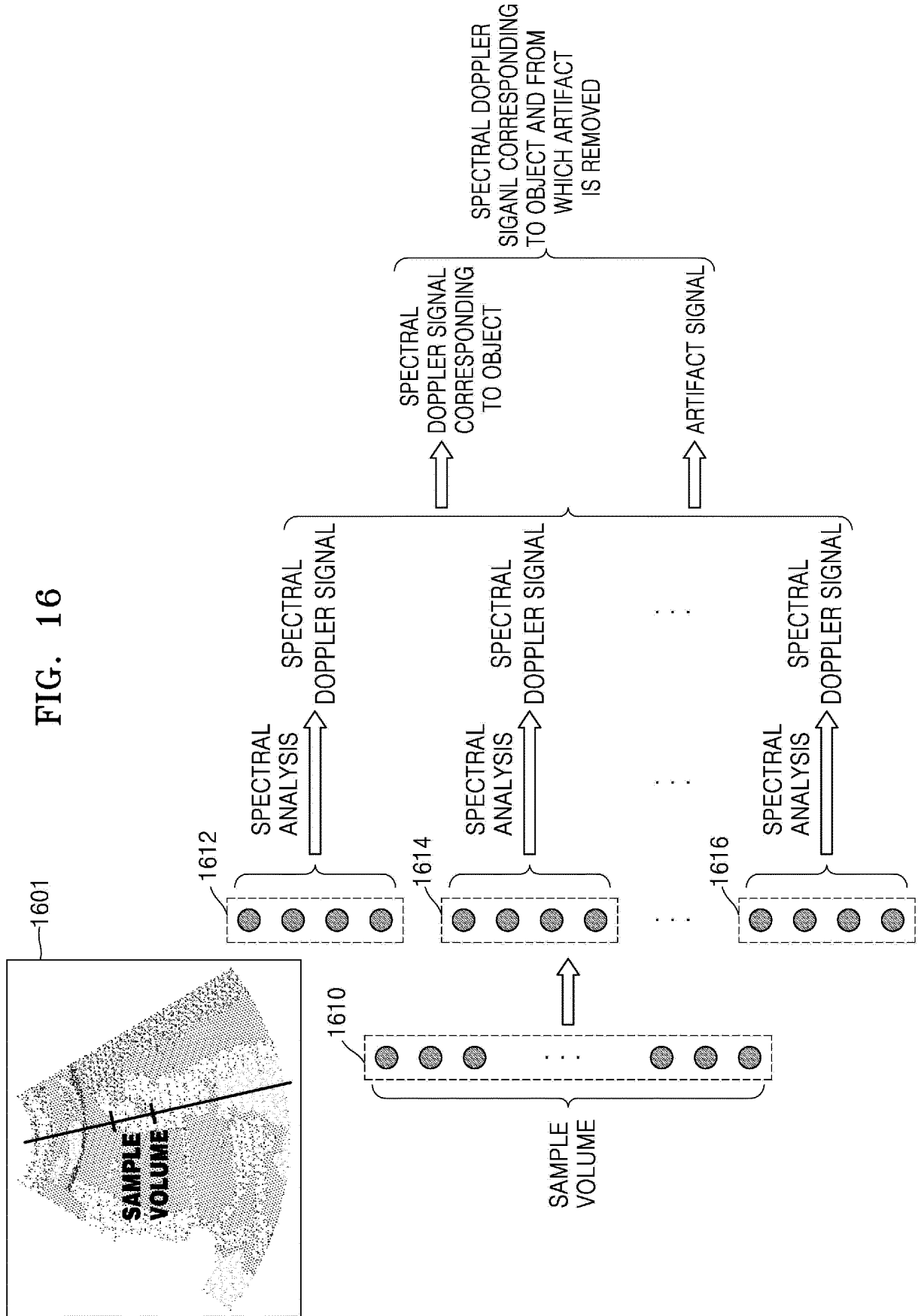


FIG. 17

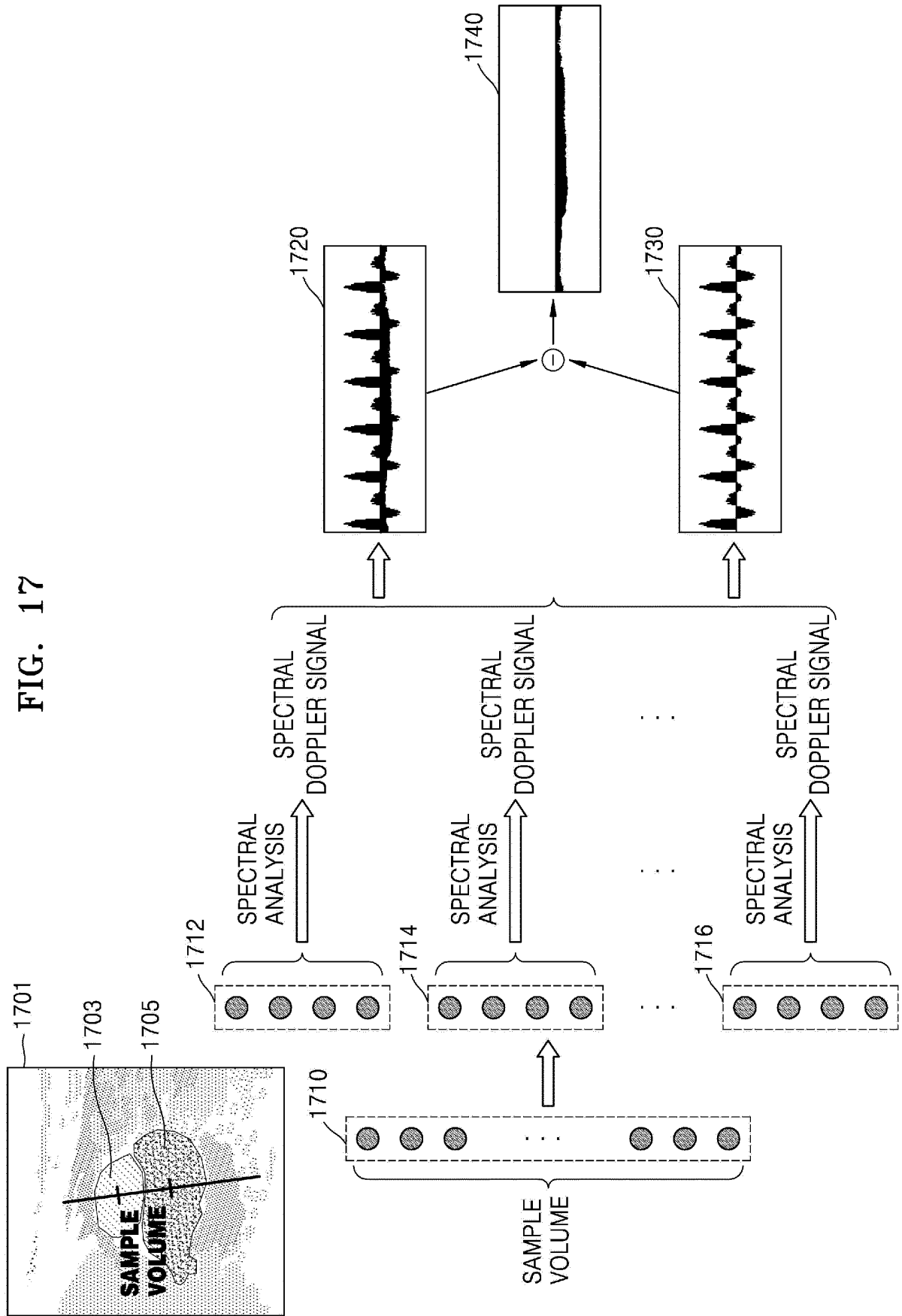


FIG. 18

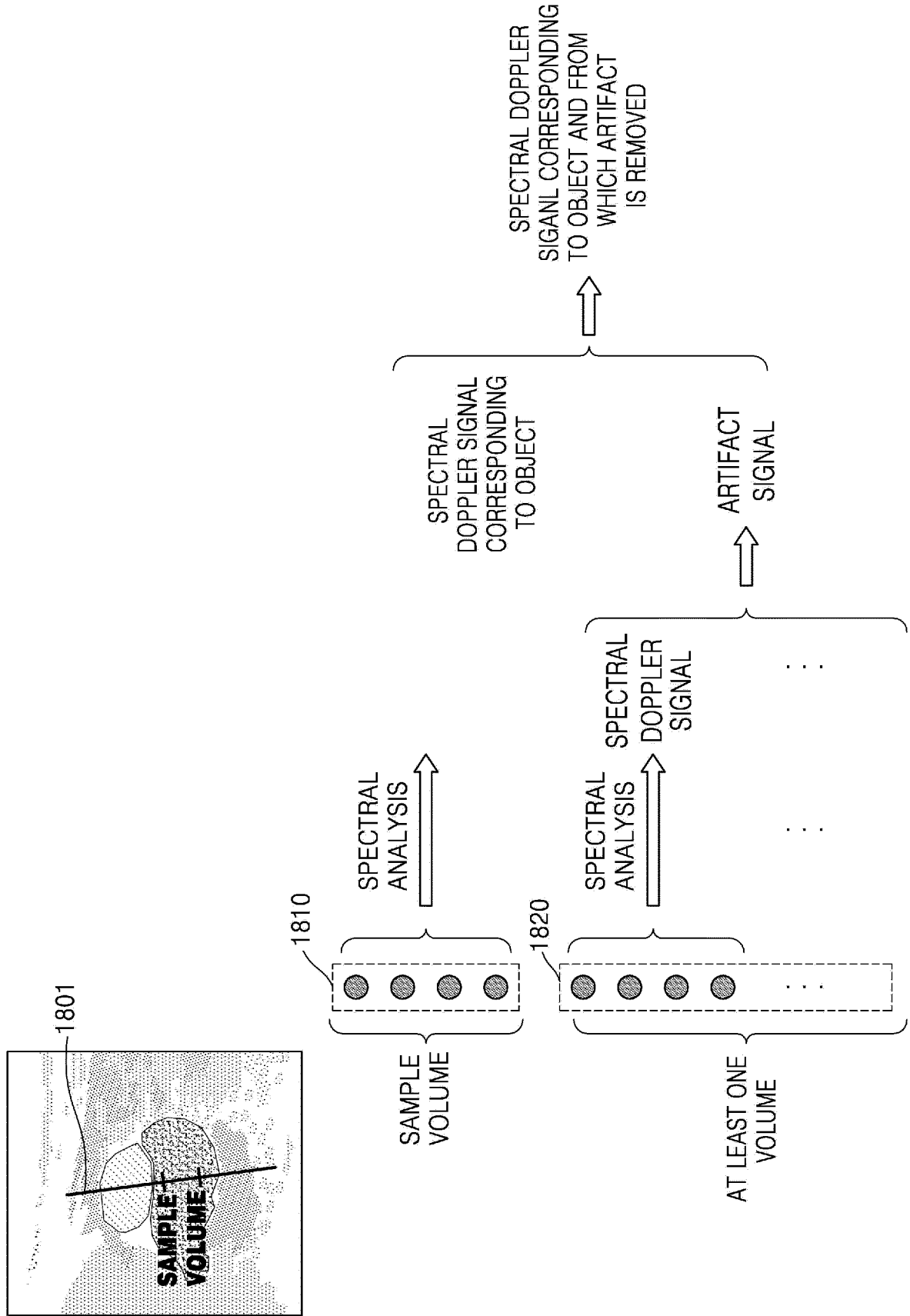
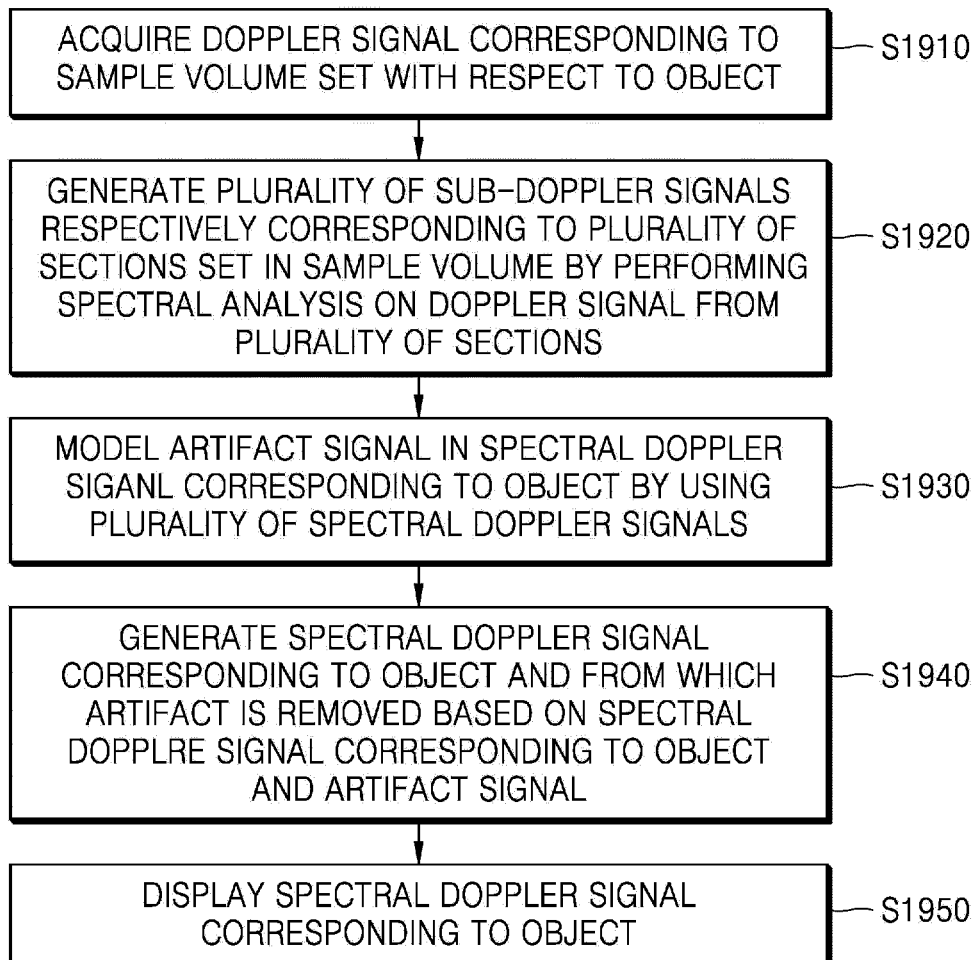


FIG. 19



INTERNATIONAL SEARCH REPORT

International application No.

PCT/KR2017/009248

A. CLASSIFICATION OF SUBJECT MATTER

A61B 8/08(2006.01)i, A61B 8/00(2006.01)i, A61B 8/06(2006.01)i

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

A61B 8/08; A61B 8/06; A61B 8/00

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Korean Utility models and applications for Utility models: IPC as above

Japanese Utility models and applications for Utility models: IPC as above

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

eKOMPASS (KIPO internal) & Keywords: ultrasonic waves, fraction, doppler, fourier transform, spectrum, weighting

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	KR 10-2010-0043686 A (MEDISON CO., LTD.) 29 April 2010 See paragraphs [16]-[27] and figures 1-3.	1-4,6,7,10-13,15
Y		5,8,9,14
Y	JP 2003-079625 A (GE MEDICAL SYSTEMS GLOBAL TECHNOLOGY CO., L.L.C.) 18 March 2003 See paragraphs [50], [68]-[86] and figures 1, 7-12.	5
Y	KR 10-2016-0094221 A (SAMSUNG MEDISON CO., LTD.) 09 August 2016 See paragraphs [50], [51] and figure 3.	8,14
Y	JP 2006-141996 A (TOSHIBA CORP. et al.) 08 June 2006 See claims 7, 8.	9
A	KR 10-2008-0084442 A (MEDISON CO., LTD.) 19 September 2008 See claim 1 and figures 3, 4.	1-15

☐ Further documents are listed in the continuation of Box C.☒ See patent family annex.

* Special categories of cited documents:

"A" document defining the general state of the art which is not considered to be of particular relevance

"E" earlier application or patent but published on or after the international filing date

"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)

"O" document referring to an oral disclosure, use, exhibition or other means

"P" document published prior to the international filing date but later than the priority date claimed

"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art

"&" document member of the same patent family

Date of the actual completion of the international search

15 DECEMBER 2017 (15.12.2017)

Date of mailing of the international search report

18 DECEMBER 2017 (18.12.2017)

Name and mailing address of the ISA/KR


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Authorized officer

Telephone No.

INTERNATIONAL SEARCH REPORT
Information on patent family members

International application No.

PCT/KR2017/009248

Patent document cited in search report	Publication date	Patent family member	Publication date
KR 10-2010-0043686 A	29/04/2010	EP 2180339 A1 JP 2010-099472 A US 2010-0099990 A1	28/04/2010 06/05/2010 22/04/2010
JP 2003-079625 A	18/03/2003	JP 3847124 B2 KR 10-0483783 B1 KR 10-2003-0024597 A US 2003-0055333 A1 US 6669642 B2	15/11/2006 20/04/2005 26/03/2003 20/03/2003 30/12/2003
KR 10-2016-0094221 A	09/08/2016	EP 3050516 A1 US 2016-0220227 A1	03/08/2016 04/08/2016
JP 2006-141996 A	08/06/2006	CN 100471456 C CN 1768709 A JP 4891590 B2 US 2006-0084873 A1 US 7513872 B2	25/03/2009 10/05/2006 07/03/2012 20/04/2006 07/04/2009
KR 10-2008-0084442 A	19/09/2008	EP 1970011 A1 EP 1970011 B1 JP 2008-229339 A JP 5366417 B2 KR 10-0961854 B1 US 2008-0228078 A1	17/09/2008 15/06/2011 02/10/2008 11/12/2013 09/06/2010 18/09/2008

专利名称(译)	超声波成像设备和超声波图像显示方法		
公开(公告)号	EP3517043A4	公开(公告)日	2020-06-10
申请号	EP2017853307	申请日	2017-08-24
[标]申请(专利权)人(译)	三星麦迪森株式会社		
申请(专利权)人(译)	三星MEDISON CO. , LTD. 西江大学研究基金会		
当前申请(专利权)人(译)	三星MEDISON CO. , LTD. 西江大学研究基金会		
[标]发明人	LEE WOO YOUL YANG EUN HO CHO GAE YOUNG KANG JIN BUM YOO YANG MO		
发明人	LEE, WOO-YOUL YANG, EUN-HO CHO, GAE-YOUNG KANG, JIN-BUM YOO, YANG-MO		
IPC分类号	A61B8/08 A61B8/00 A61B8/06		
CPC分类号	A61B8/06 A61B8/065 A61B8/08 A61B8/0891 A61B8/4405 A61B8/4427 A61B8/4472 A61B8/461 A61B8/463 A61B8/464 A61B8/467 A61B8/488 A61B8/5207 A61B8/5223 A61B8/5269 A61B8/5276 G01S7/52028 G01S7/52077 G01S15/8979		
优先权	62/396910 2016-09-20 US 62/396970 2016-09-20 US 62/396889 2016-09-20 US 1020170072725 2017-06-09 KR 1020170072726 2017-06-09 KR 1020170072727 2017-06-09 KR		
其他公开文献	EP3517043A1		
外部链接	Espacenet		

摘要(译)

提供了超声成像设备和显示超声图像的方法。 超声成像设备可以包括：处理器，被配置为获取与样本量相对应的多普勒信号，将多普勒信号划分为多个子多普勒信号，通过对多个子多普勒信号中的每个进行频谱分析来生成多个频谱多普勒信号。 子多普勒信号，并从多个频谱多普勒信号中生成与样本量相对应的频谱多普勒信号； 显示器显示对应于样本量的频谱多普勒信号。

