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(11)

EP 2 671 093 B1

(12)

EUROPEAN PATENT SPECIFICATION

(45) Date of publication and mention
of the grant of the patent:

16.01.2019 Bulletin 2019/03

(21) Application number: 12742001.6

(22) Date of filing: 31.01.2012

(51) Int Cl.:

G01S 15/89 (2006.01) **A61B 8/00 (2006.01)**
F16F 1/14 (2006.01) **G01D 5/48 (2006.01)**
G01S 7/52 (2006.01) **G01S 7/527 (2006.01)**
G01N 21/64 (2006.01) **G01N 21/65 (2006.01)**
G01N 29/14 (2006.01) **G10K 11/00 (2006.01)**

(86) International application number:
PCT/CA2012/050057

(87) International publication number:
WO 2012/103650 (09.08.2012 Gazette 2012/32)

(54) **ULTRASONIC PROBE WITH ULTRASONIC TRANSDUCERS ADDRESSABLE ON COMMON
ELECTRICAL CHANNEL**

ULTRASCHALLSONDE MIT ULTRASCHALLWANDLERN ZUR ADRESSIERUNG AUF EINEM
GEMEINSAMEN ELEKTROKANAL

SONDE À ULTRASONS COMPRENNANT DES TRANSDUCTEURS À ULTRASONS POUVANT ÊTRE
ADRESSÉS SUR UN CANAL ÉLECTRIQUE COMMUN

(84) Designated Contracting States:

**AL AT BE BG CH CY CZ DE DK EE ES FI FR GB
GR HR HU IE IS IT LI LT LU LV MC MK MT NL NO
PL PT RO RS SE SI SK SM TR**

(30) Priority: 31.01.2011 US 201161437758 P

(43) Date of publication of application:

11.12.2013 Bulletin 2013/50

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EP 2 671 093 B1

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Description

BACKGROUND

[0001] The present disclosure relates to imaging systems and probes employing ultrasonic imaging transducers. The present disclosure also relates to methods of detecting changes in the angular orientation of movable elements employed for directing radiation from imaging transducers during minimally invasive imaging procedures. High resolution biomedical imaging serves numerous purposes, including assessing tissue structures and anatomy, planning and/or guiding interventions on localized regions of the body, and assessing the result of interventions that alter the structure, composition or other properties of a region.

[0002] High frequency ultrasound, in particular, has found significant use in intracardiac and intravascular applications. For these applications, ultrasound transducers are incorporated into a catheter or other device that can be inserted into a lumen or cavity within the body. Two important implementations of high frequency ultrasound are intravascular ultrasound (IVUS) for imaging blood vessels, and intracardiac echocardiography (ICE) for imaging cardiac chambers. Both ICE and IVUS are minimally invasive, and involve placing one or more ultrasound transducers inside a blood vessel or cardiac chamber to take high quality images of these structures.

[0003] Courtney et al. (US Patent Application Publication No. US20090264768) describe an intravascular/intracardiac echocardiography catheter capable of forward viewing via 3D ultrasound and/or optical imaging. This is achieved using a movable member to image at various angles. This device benefits from knowledge of the position and/or orientation of either the imaging mechanism itself or of a deflecting element, such as a mirror.

[0004] In order to correlate the images obtained using an imaging transducer with the orientation of the imaging probe, it is important to provide a mechanism for determining the relative angular orientation of the movable portion of an imaging system. This angular orientation determines an angle at which imaging energy is transmitted and/or received from the imaging probe. Courtney et al. disclose a number of angle detection mechanisms and methods. One method involves relating the rotational speed to the imaging angle, for example, using a look-up table. A series of electronic and electromechanical techniques are also described, including capacitive, resistive, electromagnetic, inductive, and strain gauge based techniques. Also described are techniques that employ diffuse scattering from a reflector using the primary imaging source. Also disclosed are optical and acoustic methods and mechanism that utilize a detection sensor that is separate from the primary imaging source to determine the imaging angle.

[0005] There are a number of limitations related to the techniques described above. For example, the use of a lookup table relating rotational speed to imaging angle

may be prone to significant inaccuracy. Different orientations or situations may influence the relationship between imaging angle and rotational speeds. This may occur as a result of gravitational forces in different orientations, different temperature conditions, or stress on the catheter among others. Also, many techniques - predominantly those using modalities other than the imaging modality - may require the addition of significant complex components and energy sources.

5 **[0006]** Japanese Patent Publication No. 09000522 (Nobuki) discloses an ultrasonic probe configured to reduce the diameter of a catheter by placing, inside and along the longitudinal direction of the catheter, a second ultrasonic oscillator whose oscillation frequency is lower than that of a first ultrasonic oscillator, and providing a torque transfer material which transfers torque to the first and second ultrasonic oscillators.

10 **[0007]** US Patent Publication No. 2007/0016065 (Hastings et al.) discloses a phased array ultrasound **15** transducer made from a plurality of independently excitable elements that are arranged in a row in the azimuthal direction, configured so that azimuthal aiming of an outgoing ultrasound beam is controlled by timing the excitation of the elements. The geometry of the elements is **20** configured to focus the outgoing beam in the elevation direction so as to improve the images of target regions located at or about a particular radial distance. In some embodiments, this is accomplished by forming each element from a plurality of subelements that are stacked **25** in the elevation direction, with the subelements of any given element all (a) wired together and (b) positioned at about the same distance from a substantially rod-shaped focal region.

30 **[0008]** US Patent Publication No. 2009/0264768 discloses scanning mechanisms for imaging probes using **35** for imaging mammalian tissues and structures using high resolution imaging, including high frequency ultrasound and/or optical coherence tomography. The imaging probes include adjustable rotational drive mechanism for **40** imparting rotational motion to an imaging assembly containing either optical or ultrasound transducers which emit energy into the surrounding area. The imaging assembly includes a scanning mechanism having a movable member configured to deliver the energy beam **45** along a path out of said elongate hollow shaft at a variable angle with respect to said longitudinal axis to give forward and side viewing capability of the imaging assembly. The movable member is mounted in such a way that the variable angle is a function of the angular velocity of the **50** imaging assembly.

[0009] US Patent No. 6,120,455 discloses methods and apparatus for non-uniform rotation distortion detection for enhanced intravascular ultrasound imaging. The patent described methods and apparatus which detect **55** non-uniform rotation in an improved manner without using beacons which may create shadowing of tissue behind the beacons or other undesired artifacts in the image. In specific embodiments, simple and useful solu-

tions are provided for addressing the problem of non-uniform rotation distortion in intravascular ultrasound imaging in systems which use mechanical scanning. Specific embodiment utilizes correlation of received signals in an image vector from reverberating ultrasound in a bubbly liquid-flushed catheter to determine non-uniform rotation of the transducer within the catheter. Other embodiments utilize correlation of imaging vectors within a blood speckle region given a particular beamwidth of ultrasound energy from a transducer to determine non-uniform rotation of the transducer.

SUMMARY

[0010] Methods and apparatus are provided for electrically addressing multiple ultrasonic transducers that are connected to a common electrical channel and housed within an imaging probe. An imaging probe may comprise an imaging ultrasonic transducer and a moveable element for controlling the direction of an emitted imaging beam, and an angle sensing ultrasonic transducer, where the angle sensing ultrasonic transducer is configured for determining the direction of an ultrasonic imaging beam. The angle-sensing transducer may be configured to direct an angle sensing ultrasonic beam towards an acoustically reflective substrate and provide a signal by detecting a reflected ultrasonic beam reflected from the acoustically reflective substrate, where the acoustically reflective substrate is positioned relative to the movable element such that motion of the movable element produces a change in the signal.

[0011] Accordingly, in a first aspect, there is provided an imaging probe according to claim 1.

[0012] In another aspect, there is provided a method of determining a direction of an imaging beam emitted by an imaging probe according to claim 16.

[0013] A further understanding of the functional and advantageous aspects of the disclosure can be realized by reference to the following detailed description and drawings.

BRIEF DESCRIPTION OF THE DRAWINGS

[0014] Embodiments of the disclosure will now be described, by way of example only, with reference to the drawings, in which:

Figure 1 is a schematic of an imaging system including ultrasound and optical components.

Figure 2 is a perspective drawing of a flexible imaging probe with an adapter, conduit, and imaging assembly.

Figure 2a is a cross sectional view of the mid-section of the imaging probe of Figure 2 taken along the dotted line.

Figure 2b is a magnified and expanded drawing of the distal region of the imaging probe of Figure 2.

Figures 3a - 3g describe embodiments of techniques

for causing tilting of a tiltable member.

Figure 3a shows a longitudinal cutaway of a catheter in which the tilting is caused by centripetal motion. Figure 3b shows a cross-sectional cutaway of the catheter shown in Figure 3a.

Figure 3c shows the catheter of Figure 3a and the resulting tilting caused by rotating the scanning assembly at a faster rate than that of Figure 3a.

Figure 3d shows a cross-sectional cutaway of the catheter shown in Figure 3c.

Figure 3e shows a longitudinal cutaway of a catheter in which the tilting is controlled using one or more magnets.

Figure 3f shows a cross-sectional cutaway of the catheter in Figure 3e.

Figure 3g shows the catheter of Figure 3e and the resulting deflection caused by magnetism.

Figure 3h shows a cross-sectional cutaway of the catheter in Figure 3g.

Figure 3i shows a potential scanning pattern for generating 3D images with imaging angle information.

Figure 3j illustrates a control system in which the angle sensing transducer is employed to provide feedback for controlling a direction of the emitted imaging beam.

Figure 3k shows an implementation of a system using a torsional spring as a restoring mechanism.

Figure 4 demonstrates the use of a high frequency ultrasound transducer to estimate the tilt angle of a tiltable ultrasound transducer using a time of flight method. Figures 4a and 4b show the measurement of the tilt of the tiltable component at two different angular orientations. Figures 4c and 4d plot the time dependence of the transmitted and received ultrasonic pulses for the angular orientations shown in Figures 4a and 4b, respectively. Figure 4e plots the dependence of the time delay of the ultrasonic beam on the tilt angle.

Figures 5a and 5b show connection schemes of ultrasound transducers to produce acoustic energy through multiple ultrasound transducers via a single electrical connection. Figure 5a shows a case where an imaging transducer and an angle detection transducer are directly bonded together. Figure 5b shows a case where an imaging transducer and an angle detection transducer are physically separated, but connected electrically. Figures 5c-5e illustrate embodiments in which two imaging ultrasonic transducers are housed within a sheath and connected to a common electrical channel for simultaneous imaging in antiparallel (Figure 5c) and orthogonal (Figures 5d-5e), and parallel (Figure 5f). Figure 5g shows a three-frequency imaging arrangement; and Figure 5h shows an arrangement with a two-frequency assembly combined with an optical imaging modality. Figure 5i shows an arrangement with focused ultrasound transducers.

Figure 6 shows a separation between the active

bandwidths of two ultrasound transducers connected to a common channel.

Figure 7 shows the use of tuning elements for the two ultrasound transducers using separate RLC circuits for each of the transducers.

Figures 8a-8e demonstrate the use of a high frequency ultrasound transducer to estimate the deflection of a tiltable optical and/or acoustic mirror. Figures 8a and 8b show the measurement of the tilt angle of the tiltable mirror at two different angular orientations. Figures 8c and 8d plot the time dependence of the transmitted and received ultrasonic pulses for the angular orientations shown in Figures 8a and 8b, respectively. Figure 8e plots the dependence of the time delay of the ultrasonic beam on the deflection angle.

Figures 9a-9e demonstrate the use of a high frequency ultrasound transducer to estimate the angular orientation of an ultrasound transducer mounted on a deformable member. Figures 9a and 9b show the measurement of tilt of the mirror at two different angular orientations. Figures 9c and 9d plot the time dependence of the transmitted and received ultrasonic pulses for the angular orientations shown in Figures 9a and 9b, respectively. Figure 9e plots the dependence of the time delay of the angle detecting ultrasonic beam on the tilt angle.

Figures 10a-10e demonstrate the use of a high frequency ultrasound transducer to estimate the deflection angle of a tiltable component using a method that assesses the intensity of the received signal. Figures 10a and 10b show the measurement of the tilt of a tiltable component at two different angular orientations. Figures 10c and 10d plot the time dependence of the transmitted and received ultrasonic pulses for the angular orientations shown in Figures 10a and 10b, respectively. Figure 10e plots the dependence of the peak voltage relating to the received ultrasonic beam on the deflection angle.

Figures 11a and 11b show (a) the use of a surface comprising a specular reflector in comparison with (b) a diffuse reflector. Figures 11c and 11d plot the time dependence of the transmitted and received ultrasonic pulses for the angular orientations shown in Figures 11a and 11b, respectively.

Figures 12a-d demonstrate the use of two high frequency ultrasound transducers to estimate the deflection angle of a tiltable component using a time of flight method, shown in (a) and (b) at two different angular orientations. Figures 12c and 12d plot the time dependence of the transmitted and received ultrasonic pulses for the angular orientations shown in Figures 12a and 12b, respectively.

Figures 13a-e show a disc with curved features to increase the range of angles that can be detected using a time of flight method, shown in (a) and (b) at two different angular orientations. Figures 13c and 13d plot the time dependence of the transmitted and

received ultrasonic pulses for the angular orientations shown in Figures 13a and 13b, respectively. Figure 13e plots the dependence of the time delay of the ultrasonic beam on the deflection angle.

Figures 14a-d show the use of an ultrasound transducer that diffusely emits and detects ultrasound energy to increase the range of angles that can be detected using a time of flight method, shown in (a) and (b) at two different angular orientations. Figures 14c and 14d plot the time dependence of the transmitted and received ultrasonic pulses for the angular orientations shown in Figures 14a and 14b, respectively. Figures 15a-d show the use of a curved surface to increase the range of angles that can be detected with improved precision using a time of flight method with an angle detection transducer attached to a tiltable component, shown in (a) and (b) at two different angular orientations. Figures 15c and 15d plot the time dependence of the transmitted and received ultrasonic pulses for the angular orientations shown in Figures 15a and 15b, respectively. Figure 15e illustrates the relationship between the curvature of the surface and the orientation of the transducer, such that the surface is locally approximately normal to the incident acoustic beam to ensure strong received signals.

Figures 16a-d show the use of a high frequency ultrasound transducer to estimate the tilt angle of a tiltable ultrasound transducer mechanically coupled to an otherwise acoustically passive component with the angle detection transducer mounted on the otherwise acoustically passive component, shown in Figures 16a and 16b at two different angular orientations. Figures 16c and 16d plot the time dependence of the transmitted and received ultrasonic pulses for the angular orientations shown in Figures 16a and 16b, respectively. Figure 16e shows some geometric relationships that can be used to calculate the tilt angle from the knowledge of the distance between angle detection transducer and a constant distance between a point on each of two tiltable components.

Figures 17a-d show the use of a high frequency ultrasound transducer to estimate the deflection angle of a tiltable ultrasound transducer mechanically coupled to an acoustically passive component with an angle detection transducer integrated onto an imaging transducer. Figures 17c and 17d plot the time dependence of the transmitted and received ultrasonic pulses for the angular orientations shown in Figures 17a and 17b, respectively.

Figures 18a-b show the use of the curved surface shown in Figure 15 with a mechanically coupled acoustically passive component similar to that shown in Figures 16 and 17. Figure 18a shows a view with the same perspective shown in Figure 17. Figure 18b shows a view cut through the hatched line from Figure 18a.

Figures 18c-18i show an embodiment in which the position of the mechanical coupler is detected using the angle detection transducer to estimate the angle of deflection. Figures 18c and 18e show the tiltable member at two different positions. Figures 18d and 18f show views cut through the hatched line from Figures 18c and 18e respectively. Figures 18g and 18h show timing diagrams from the scenarios described in Figures 18d and 18f respectively. Figure 18i shows a relationship between the received time delay and the tilt angle.

Figures 19a-g show a sample pulse sequence and corresponding received signal from both the imaging transducer and the deflection angle transducer on a single channel using multiple methods. Figure 19a shows the measurement of two features, and Figure 19b shows how the signals from the two features and the signal from the angle detection transducer can be extracted based on an interleaved pulsing scheme.

Figure 19c shows an example using either or both of: prior knowledge of distance ranges and using spectral methods. Figure 19d shows how the signals from the two features and the signal from the angle detection transducer can be extracted based on whether or not they are beyond the maximum distance range used in the angle detection scheme. Figures 19e shows an example of the use of spectral methods to separate angle detection information from imaging information.

Figure 19f shows a transmit pulse sequence where multiple imaging pulses are transmitted between single angle detection pulses. Figure 19g shows a transmit pulse sequence where there is a long time delay between the imaging pulse and the subsequent angle detection pulse, and a short time delay between the angle detection pulse and the subsequent imaging pulse.

Figures 20a-b show different estimation methods for determining a distance as detected by an angle detection transducer. Figure 20a shows an example of the detection of the distance based on the use of radio-frequency (RF) peak detection methods and envelope detection methods, while Figure 20b example illustrates the detection of the distance based on the use of cross correlation methods.

Figure 21 shows experimental data obtained from an angle detection experiment conducted with the embodiment described in Figure 18a and 18b.

DETAILED DESCRIPTION

[0015] Various embodiments and aspects of the disclosure will be described with reference to details discussed below. The following description and drawings are illustrative of the disclosure and are not to be construed as limiting the disclosure. Numerous specific details are described to provide a thorough understanding

of various embodiments of the present disclosure. However, in certain instances, well-known or conventional details are not described in order to provide a concise discussion of embodiments of the present disclosure. It should be understood that the order of the steps of the methods disclosed herein is immaterial so long as the methods remain operable. Moreover, two or more steps may be conducted simultaneously or in a different order than recited herein unless otherwise specified.

[0016] As used herein, the terms, "comprises" and "comprising" are to be construed as being inclusive and open ended, and not exclusive. Specifically, when used in the specification and claims, the terms, "comprises" and "comprising" and variations thereof mean the specified features, steps or components are included. These terms are not to be interpreted to exclude the presence of other features, steps or components.

[0017] As used herein, the term "example" means "serving as an example, instance, or illustration," and should not be construed as preferred or advantageous over other configurations disclosed herein.

[0018] As used herein, the terms "about" and "approximately", when used in conjunction with ranges of dimensions of particles, compositions of mixtures or other physical properties or characteristics, are meant to cover slight variations that may exist in the upper and lower limits of the ranges of dimensions so as to not exclude embodiments where on average most of the dimensions are satisfied but where statistically dimensions may exist outside this region. It is not the intention to exclude embodiments such as these from the present disclosure. For example, in embodiments of the present disclosure, dimensions of components of the imaging probe are given but it will be understood that these are not meant to be limiting.

[0019] As used herein, the term "high resolution imaging" generally refers to optical imaging methods and high frequency ultrasound, the latter of which typically involving frequencies of greater than 3 MHz, and more typically involving frequencies in the range of 5 to 100 MHz.

[0020] As used herein, the terms "imaging radiation" and "imaging energy" refer to electromagnetic or acoustic radiation, or both. Specifically, electromagnetic radiation may span the ultraviolet, visible, and or infrared spectrum of wavelengths.

[0021] As used herein, the term "deflect" refers to a change in at least an angular orientation of an object relative to. In one example, a deflection may be a change in the tilt of a tiltable component or a change in an angular orientation of a movable member. As used herein, the term "tilt" refers to the angular orientation of an object. A change in angular orientation, as defined by a change in a tilt angle, may be relative to another portion of an object if the object is deformable, or relative to another object within an assembly of objects. For example, a component mounted on a pivot mechanism may tilt by pivoting around an axis of the pivot mechanism. Alternatively, a component mounted on a deformable component or in-

tegrated as part of a deformable component may experience a tilt as a result of deformation of the deformable component.

[0022] As used herein, the term "move" refers to a change in either an angular orientation of an object, a position of an object or both the angular orientation and position of an object. For example, the movement of an object may occur as a result of a tilting an object or pivoting of an object around an axis. Movement may also occur as a result of a deformation an object or a deformable portion of an object. Movement may also occur as a result of translation of an object. The movement of an object may be in absolute terms, relative to another portion of an object if the object is deformable, or relative to another object within an assembly of objects.

[0023] As used herein, the term "electrical channel" refers electrically conductive paths that are suitable for delivering electrical energy to, or detecting electrical signals from, an electrical element, such as an ultrasonic transducer. An example of an electrical channel includes two conductors, such as wires, that are contacted with an electrical element such that when a voltage difference is applied between the conductors, a corresponding voltage is applied across the electrical element.

[0024] Embodiments of the disclosure provide apparatus and methods for the non-contact detection of a change in orientation or position of a movable member. An ultrasonic transducer is employed to generate an incident ultrasonic beam and to detect a reflected ultrasonic beam, where the deflection of a deflectable member produces a change in one or more of: a) the intensity, b) the time delay, or c) the spectral content of the reflected beam. The proceeding disclosure describes and illustrates, through examples, the application of various embodiments to minimally invasive imaging systems and methods. However, it is to be understood that these applications are merely non-limiting examples, and the embodiments disclosed here are applicable and adaptable to a wide range of uses and applications.

[0025] Before describing example embodiments and their application to minimally invasive imaging systems, a brief review of minimally invasive imaging systems is provided with reference to Figures 1 to 3, by way of example. Referring first to Figure 1, an imaging system is shown at 10 comprising imaging probe 44, which connects via patient interface module 36 to image processing and display system 49. Image processing and display system 49 includes hardware to support one or more imaging modalities, such as ultrasound, optical coherence tomography, angioscopy, infrared imaging, near infrared imaging, Raman spectroscopy-based imaging, or fluorescence imaging. Specific embodiments of ultrasonic imaging probes and combined ultrasonic and optical imaging probes are disclosed by Courtney et al. in US Patent Publication No. 20080177183, titled "Imaging Probe with Combined Ultrasounds and Optical Means of Imaging" and filed on January 22, 2008, US Patent Publication No. 20080177138, titled "Scanning Mechanisms

for Imaging Probe" and filed on January 22, 2008 and US Patent Publication No. 20090264768, titled "Scanning Mechanisms for Imaging Probe" and filed on March 27, 2009.

[0026] Controller and processing unit 34 is employed to facilitate the coordinated activity of the many functional units of the system, and may contain some or all of the components shown in the Figure and listed herein. An operator interacts with system 50 via display and/or user interface 38. System 10 may further include electrode sensors 40 to acquire electrocardiogram signals from the body of the patient being imaged. The electrocardiogram signals may be used to time the acquisition of imaging data in situations where cardiac motion may have an impact on image quality. The electrocardiogram may also serve as a trigger for when to begin an acquisition sequence, such as when to begin changing the speed of rotation of a motor in order to cause a desired scan pattern to take effect. For example, electrocardiogram triggered initiation of an imaging sequence may enable images to be acquired during a particular phase of the cardiac cycle, such as systole or diastole.

[0027] Optical subsystem 30, if included in a particular implementation of an imaging system, may include any or all of the following components: interferometer components, one or more optical reference arms, optical multiplexors, optical demultiplexers, light sources, photodetectors, spectrometers, polarization filters, polarization controllers, timing circuitry, analog to digital converters, parallel processing arrays and other components known to facilitate any of the optical imaging techniques. Ultrasound subsystem 32 may include any or all of the following components: pulse generators, electronic filters, analog to digital converters, parallel processing arrays, envelope detectors, amplifiers including time gain compensation amplifiers and other components known to facilitate acoustic imaging techniques.

[0028] Controller and processing units 34, if included in a particular implementation of the imaging system, serve multiple purposes. Those skilled in the art will appreciate that specific components required depend on the needs of a particular type of imaging system. For example, controller and processing units may include any combination of a motor drive controller, data storage components (such as memory, hard drives, removable storage devices, readers and recorders for media such as CDs, DVDs, and Bluray™ discs), position sensing circuitry and/or software, angle detection circuitry and/or software, timing circuitry and/or software, cardiac gating functionality, volumetric imaging processors, scan converters and others. As noted above, display and user interface 38 is also optionally provided for either real time display or display of data at a time later than the time at which imaging data is acquired.

[0029] It is to be understood that patient interface module 36 and controller and processing units 34 are but one example illustration of the selection and organization of hardware subsystems, and that many other implemen-

tations are possible. For example, patient interface module 36 may be housed with controller and processing units 34 within processing and display system 49.

[0030] Example imaging probe 44 includes an imaging assembly 50, optional imaging conduit 46 along a substantial portion of its length, and connector 48 at its proximal end 47. Imaging assembly 50 is located near distal end 41 of imaging probe 44. Imaging assembly 50 generally refers to the components of the imaging probe 44 from which the signals (either acoustic, optical or both) are collected for the purposes of imaging a region that is proximate to imaging assembly 50. Imaging assembly 50 may house transducers for transmitting and/or receiving imaging radiation. The emitter and receiver may be a single component, as is often the case with a piezoelectric transducer.

[0031] In the case of optical imaging, imaging assembly 50 typically contains the distal tip of a fiber optic, as well as a combination of optical components such as a lens (for instance, a ball lens or a GRIN lens). A mirror and/or prism may be included for use in beam delivery and/or collection. Optionally, there may be an optical detector, such as a CCD array, or an optical light source, such as one or more LEDs, incorporated directly in the imaging assembly that may obviate the need for one or more fiber optics in an optical imaging probe.

[0032] Imaging probe 44 may contain ports at one or more points along its length to facilitate flushing. Moreover, imaging assembly 50, connector 48 and/or imaging conduit 46 may be filled and / or surrounded with a fluid such as saline, and may be flushed. In applications involving optical imaging, imaging probe 44 may be filled with a gas. The gas may include carbon dioxide or another readily dissolved gas with minimal biotoxicity. Alternatively, in the case of a multimodal optical/acoustic imaging system, imaging assembly 50 may be compartmentalized to include at least one gas-filled compartment or lumen for optical imaging and at least one fluid filled compartment or chamber for acoustic imaging.

[0033] Imaging conduit 46 includes at least one conductive wire (optionally two or more) that connect an emitter and/or receiver via connection to an adapter, herein referred to as patient interface module 36. Imaging conduit 46 may include a fiber optic, for example, wrapped by two layers of electrical wire that are electrically insulated from one another. Imaging conduit 46 may further be reinforced by other structural features, such as helically wrapped wires or other designs used to construct imaging torque cables for rotating scan mechanisms. Alternatively, imaging conduit 46 may contain electrical conductors, and a rotational mechanism may be located remote from the proximal end for imparting rotary motion to the imaging assembly. One example mechanism includes a micro-motor and a slip ring in close proximity to the imaging assembly.

[0034] The imaging probe 44 may optionally include memory, such as an EEPROM for storing information including calibration information, serial information,

probe design information, desired filter information, and any other probe specific information. This memory may reside in connector 48.

[0035] Patient interface module 36 facilitates transmission of signals within any fibers and/or wires to the appropriate image processing units. It may contain a motor drive unit for imparting rotational motion to the components of the imaging mechanism.

[0036] Additional sensors may be incorporated as part of patient interface module 36, such as position sensing circuitry, for example, to sense the angle of rotation of a rotary component within the imaging probe 44 and/or for detecting the angle of deflection of a member at the distal end 41 of the imaging probe 44. Additionally, patient interface module 36 may include amplifiers to improve the transmission of electrical signals or power between the imaging probe 44 and the rest of the system.

[0037] In many applications, it can be important to optimize the geometry of a minimally invasive probe so that it is as small as reasonably possible to achieve its desired purpose. Current IVUS and ICE probes are approximately 0.9 to 4 mm in diameter and the smaller sizes of probes can be delivered more distally within the vascular tree of the coronary anatomy as the vessel caliber tapers down or as diseased vessels are stenosed. Furthermore, within the cardiac anatomy, smaller probes (such as those with a diameter less than about 3.4 mm) can be readily advanced across the atrial septum into the left atrium of the heart. Thus, smaller sizes generally allow for interrogation of a larger portion of the coronary or cardiac anatomy. It is therefore desirable for a probe and its components to be contained within a minimal outer diameter to enable imaging, such as using imaging performed with the scanning mechanisms described by Courtney et al. (US Patent Application Publication No. 20080177138).

[0038] Figure 2 is a perspective drawing of a flexible catheter containing fiber optic 66 and co-axial electrical cable 68. The proximal connector contains fiber optic connection joint 60 that can be received by patient interface module 36 to optically couple imaging fiber optic 66 to image processing and display system 49. Electrical connectors 62 allow one or more electrical conduits to be connected to the ultrasound circuitry and/or controller and processing units. In applications in which the imaging conduit rotates around its longitudinal axis, there may be a need to couple the rotating components of the imaging fiber optic with a relatively stationary fiber optic that connects to image processing and display system 49. This coupling can be achieved with the use of a fiber optic rotary joint incorporated either as part of the proximal connector of imaging probe 48 or as part of patient interface module 36. Similarly, there may need to be a mechanism for coupling the rotating components of the electrical system with relatively stationary electrical components that connect to image processing and display system 49. This can be achieved through the use of one or more electrical slip rings or slip ring channels.

[0039] Figure 2a shows a cross sectional view of the

middle section of the catheter shown in Figure 2 taken along the dotted vertical line. The cross section shows the optional fiber optic 66, optional guidewire 52, imaging conduit lumen 47, external sheath 43, which is a hollow, flexible elongate shaft made of physiologically compatible material and having a diameter suitable to permit insertion of the hollow elongate shaft into bodily lumens and cavities, and co-axial wiring 68. The expanded detailed view of the end of the imaging probe 44 in Figure 2b shows the imaging assembly 50 which optionally includes a tiltable member 51, distal end of the optional guidewire 52 extended beyond the end of the external sheath 43 and a flush port 53 near the end of the sheath 43. In Figure 2, the proximal end of the imaging probe 44 includes an optional guidewire port 56 into which the guidewire 52 is inserted and the connector assembly 48 includes a flush port 58 and electrical contacts 62 along with the connector body. An optional guidewire port 54 is seen in Figure 2b.

[0040] Figures 3a-d show an example catheter that employs a tiltable member for scanning an imaging beam. Figure 3a shows a perspective cutaway drawing of the distal region of an imaging probe 44 that relies on centripetal force to generate the change in tilt angle of the tiltable member 51. Imaging probe 44, which includes a sheath 43 for isolation from bodily fluids and cavities, includes tiltable member 51 housed within imaging assembly 50.

[0041] Tiltable member 51 is mounted on pins 102, about which tiltable member 51 is free to pivot. As imaging conduit 46 and assembly 50 (not shown) are rotated about longitudinal axis 59 at a slow rate (indicated by arcing hatched arrow 61), the angle α subtended between longitudinal axis 59 and tiltable member 51 is relatively small. A cutaway perspective cross-sectional view of Figure 3a is shown in Figure 3b. Figure 3c shows a similar drawing of the distal region of imaging probe 44 as shown in Figure 3a, except with imaging conduit 46 being rotated at a faster rate (indicated by arcing hatched arrow 63) than in Figure 3a. Centripetal force causes tiltable member 51 to tilt such that there is an increase in the angle α subtended between the longitudinal axis of the catheter and the tiltable member 51. Figure 3d is a cutaway perspective cross-sectional view from Figure 3c.

[0042] Figure 3e shows a perspective cutaway drawing of the distal region of a related imaging probe 44 that relies on the use of dynamically controlled magnetic fields to change the deflection angle of tiltable member 51. Imaging probe 44, which may include a sheath 43 for some degree of isolation from bodily fluids and cavities, includes tiltable member 51 comprising part of the imaging assembly 50. Tiltable member 51 is mounted on pins 102, about which the tiltable member 51 is free to pivot. Mounted on the tiltable member 51 is a magnetically influenced element 109 that can be either attracted or repulsed by a magnetic field. For example, it may be a ferromagnetic component, or a permanent magnetic

component. Element 109 may integrally be part of tiltable member 51, such as if all or a portion of element 109 is made of either a ferromagnetic or magnetic substrate. An electromagnetic component 107 is also placed at a position separate from the tiltable member 51. The electromagnetic component can be controlled to produce attractive or repulsive forces relative to magnetically influenced component 109. In so doing, the angle α subtended between the longitudinal axis 59 of the catheter and the tiltable member can be adjusted as desired. Furthermore, similar imaging probes may be conceived that involve interchanging the position of the electromagnetic component 107 and magnetically influenced component 109, or using two electromagnets instead of an electromagnet and a magnetically influenced component. A cut-away perspective cross-sectional view of Figure 3e is shown in Figure 3f.

[0043] Figure 3g shows a similar drawing of the distal region of imaging probe 44 as shown in Figure 3e, except with a repulsive sequence applied to electromagnet 107 such that the angle α subtended by tiltable member 51 is increased. Figure 3h is a cutaway perspective cross-sectional view from Figure 3g.

[0044] Tiltable member 51 may be an ultrasonic transducer, such as an ultrasound transducer used for producing B-scan ultrasound images. Another embodiment includes an ultrasound transducer mounted on a tiltable member.

[0045] Figure 3i shows an example of a potential scanning pattern for generating ultrasound images. In this case, the tiltable member is an ultrasound imaging transducer 101. As imaging conduit 46 and assembly 50 are rotated at a constant rate, an image is generated along a surface that approximates a cone. As the rate of rotation is changed, centripetal force causes the angle subtended between the longitudinal axis of the catheter and ultrasound imaging transducer 101 to change resulting in a series of concentric imaging cones 118 for different rotational speeds. The angle subtended between the longitudinal axis of the catheter and an axis normal to ultrasonic imaging transducer 101 will be referred to as the "imaging angle". In this case, the transducer begins with a relatively small imaging angle θ_1 implying a fast rate of rotational speed. As the rotational speed is reduced, the imaging angle is increased to θ_2 .

[0046] In order to cause the imaging angle to return to a stable position in the absence of rotation, a restoring mechanism can be used as shown in Figure 3k. Here, the primary movable member 101 is connected to a secondary movable member 114 using a mechanical coupler 176, allowing the two members 101 and 114 to move synchronously. All components are housed within a shell 178. One or more springs 182 are connected between the movable member 101 and the shell 178. The springs 55 may be torsion springs, linear springs, or a cantilever spring. The movable members 101 and 114 are pivotally supported by around pins 111 and 113 respectively. This spring 182 provides a force to restore the member 101

to the side viewing position in the absence of adequate rotational force to overcome the restoring force provided by spring 182. In addition to adding a mechanical restoring force, the torsional springs may also be formed, at least in part, from an electrically conductive material, such as stainless steel, beryllium copper, copper, silver, titanium, gold, platinum, palladium, rhenium, tungsten, nickel, cobalt, alloys that include one or more of these metals and many other metals and their alloys can be used to provide electrical connections. Here, spring 182 is in electrical communication with conductor 300. Conductor 301 makes a similar connection to the opposite side of movable member 101 (not shown).

[0047] Alternatively a spring that provides both a restoring force and an electrical connection may be made of more than one material, where one material provides conductive properties and another material provides mechanical properties for the restoring force. For example, a torsion spring may be formed of a nitinol core with a gold outer layer, applied by sputtering, plating, evaporation, electroforming, electroplating, electron beam techniques or other methods known in the art. Alternatively, one or more of the materials may be a material other than a metal, such as a polymer.

[0048] The conducting elements of the spring have cross sectional dimensions on a micron scale (for example, less than about 100 microns x 100 microns) using photolithography and related techniques. Gold hardened with cobalt and nickel cobalt provide further examples of suitable materials for a conductive spring with desired mechanical properties. A portion of the surface of the spring may be covered by an insulating material, such as parylene, Teflon, polyimide and many others. Alternatively, the insulating may occur by processing the outer surface of the spring, such as by allowing an oxide to form on the outer surface of a metal or alloy.

[0049] Example embodiments described below provide ultrasonic apparatuses and methods for combining multiple ultrasound transducers on a single electrical channel. One application that will be described in detail relates to the fact that in order to accurately reconstruct a 3D image of the imaging field, the imaging angle must be determined for a given ultrasound image acquisition event, vector, or pixel. As noted above, while the proceeding embodiments relate to applications involving minimally invasive imaging, where angular detection is performed using an apparatus mounted within an imaging assembly within an imaging probe, it is to be understood that these applications are merely non-limiting examples that are provided for teaching purposes and are not intended to limit the scope of the disclosed embodiments.

[0050] Referring now to Figure 4, an ultrasonic angle detection apparatus is shown for detecting a change in angle of a tiltable member using a time of flight detection method. Angle detection transducer 100 is placed at a fixed location relative to an initial position of tiltable member 101, which includes material that is at least partially

acoustically reflective relative to the acoustic transmission medium. Angle detection transducer 100 transmits ultrasonic beam 110 towards the tiltable member 101. As the beam reaches the tiltable member 101, a portion of the beam is reflected back towards the angle detection transducer 100. The acoustically reflective substrate may be configured to reflect or scatter components of the incident ultrasonic beam in a diffuse manner, as will be described in further detail below.

[0051] Tiltable member 101 may itself be acoustically reflective, or may have attached to one or more of its surfaces, such as its back surface, an acoustically reflective substrate. As noted above, acoustic reflections may be diffuse to support the detection of a reflected ultrasonic beam over a broad range of tilt angles (or imaging angles), and the reflected ultrasonic beam may be generated by surface reflection, volume reflection, or a combination thereof. In an example embodiment, tiltable member 101 includes an imaging transducer that transmits an acoustic beam 120 in a direction away from the angle detection transducer 100. It is not necessary that the angle detection mechanism only uses the back surface of the tiltable member. It may be oriented and /or positioned to use any side or surface of the tiltable member as best suited for any particular embodiment.

[0052] Figures 4a and 4b show two different angular positions of tiltable member 101, which is rotatable about pivot axis 102. In one example embodiment, the pivot axis is implemented using one or more pins or a hinge aligned along the pivot axis around which the tiltable member pivots. In Figure 4a, the separation between tiltable member 101 and angle detection transducer 100 is greater than in Figure 4b. This separation distance results in the angle detection beam 110 having a shorter time of flight in Figure 4b than Figure 4a.

[0053] The tilt angle can be calculated with the time of flight and prior knowledge of the geometric configuration of the transducer and the tiltable component, including their relative locations in space and ranges of motion, and the speed of sound in the acoustic path. The acoustic beam for the angle detection transducer may travel through a medium such as water or saline, wherein the speed of sound is approximately 1450 to 1600 m/s.

[0054] For example, if the angle is to be determined based on differences in time of flight, a baseline signal may be captured at a known angular position and known estimated time of flight during an initialization phase. This baseline signal may be used as a comparator against signals received at different positions to estimate tilt angle using the techniques described above.

[0055] Alternatively, the tilt angle can be determined empirically based on calibration measurements made with known angular deflections. Calibration measurements can be employed to produce a calibration curve, such as the curve shown in Figure 4e. Such calibration data may be stored in an EEPROM provided within the imaging probe, as described above.

[0056] Figures 4c and 4d are timing diagrams that rep-

resent the signal detected for each angle scenario in Figures 4a and 4b, respectively. In these examples, a pulse 500 is transmitted from transducer 100 at time (t) = 0 and a received pulse is detected at a later time with a reduced magnitude. The received pulse 502 corresponding to the signal reflected from tiltable member 101, as oriented in Figure 4a, has a greater time delay than the received pulse 504 corresponding to the signal reflected from tiltable member 101 in Figure 4b. Furthermore, as acoustic waves propagate through a medium, they are partially attenuated. This attenuation is frequency dependent with energy components in the higher frequencies attenuated more than lower frequency energy components. As a result of this, not only is the delay between received pulses changed, so too is the spectral content of the received pulse 504. In this embodiment, a change in spectral content can also be related to the tilt angle.

[0057] The tilt angle determined using the above method may be employed for feedback in a control system, as shown in Figure 3j. A desired angle 194 and the measured angle 192 (determined using the aforementioned method) are provided as inputs to controller 196, and the output of controller 196 is provided to angle control mechanism 190. A variety of control methods and algorithms known in the art may be employed, including, but not limited to, PID and fuzzy logic controllers.

[0058] In another example embodiment, the tiltable member is employed to direct a beam of ultrasonic radiation from an imaging ultrasonic transducer housed within an imaging probe, where the ultrasonic imaging transducer and the angle sensing transducer are electrically connected to a common channel for excitation and detection. The ultrasonic imaging transducer may form tiltable member 101, or alternatively may be mounted to tiltable member 101, or may be fixed relative to tiltable member 101 such that the imaging beam is reflected, scattered, and/or refracted by tiltable member 101 (as shown in embodiments described below).

[0059] By connecting both transducers to a common electrical channel, a simple, reliable, cost-effective, and space efficient system is realized. Furthermore, the ability to use a common electrical channel may minimize the number of electrical connections that need to be made. For example, if the electrical connections to an ultrasound imaging transducer mounted on or incorporated as tiltable member 101 are via wires or conductive springs from the housing of imaging assembly 50 to tiltable member, the wires or springs will mechanically influence the ease with which tiltable member can tilt. It may be desirable to minimize the number of wires or springs between tiltable member 101 and the rest of the imaging assembly 50.

[0060] Using a common electrical channel for both an imaging transducer and an angle detection transducer reduces the number of electrical conductors to the tiltable member and may thus provide more flexibility in the design and /or performance of the imaging probe. Similarly, using a common electrical channel may reduce the

number of channels that need to be accommodated by the patient interface module 36 (the patient interface module contains components, such as slip rings, that couple electrical signals between the rotating parts of the imaging probe and the non-rotating parts of the image processing and display system 49). Similarly, using a common electrical channel may reduce the number of analog to digital converters or reduce the number or complexity of other signal processing components in the image processing and display system 49.

[0061] Furthermore, a common electrical channel may help optimize the size, configuration and / or number of electrical conductors in the imaging conduit. This would potentially improve the mechanical properties of the imaging conduit 46, such as improving the flexibility of the imaging conduit, reducing the amount of non-uniform rotational distortion, reducing the required size of the imaging conduit 46 or providing room for additional features to be incorporated into imaging probe 44.

[0062] It is to be understood that the present embodiments pertaining to the connection of two or more ultrasonic transducers on a common electrical channel are not intended to be limited to applications involving the use of one imaging transducer and one angle detection transducer. As further described below, the common electrical connection of multiple ultrasonic transducers within a longitudinal body of an ultrasonic probe may be implemented in a wide variety of applications, for which imaging and angle detection are illustrative yet non-limiting embodiments.

[0063] Figures 5a and 5b provide schematics illustrating two example embodiments in which a single electrical channel is employed within imaging conduit 46 as a source for both an imaging transducer 105 in the imaging probe 44 and a second transducer, such as an angle detection transducer 100.

[0064] Figure 5a shows the distal end of coaxial cable 302, where first and second conductive paths 300 and 301 are connected in parallel to ultrasonic imaging transducer 105 and ultrasonic angle detecting transducer 100. For minimally invasive imaging procedures, electrical cable 302 may be a micro-coaxial cable or micro twisted pair with a diameter of less than about 1000 microns, or alternatively less than 500 microns. Excitation pulses are transmitted to both ultrasonic transducers along signal wire 301, while a second connection, optionally to ground, is provided by second wire 300. The conductive paths of the channel, labeled as the signal (+) and ground (GND) paths may be interchanged. Both transducers are shown in a side view.

[0065] Imaging transducer 105 may be larger in size than angle sensing transducer 100, and imaging transducer 105 may possess a lower center frequency than angle sensing transducer 100. In one example implementation, the center frequency of imaging transducer 105 may be in the range of 5-60MHz, while the center frequency of angle detection transducer 100 may be in the range of 25-100MHz. In another example embodiment,

ment, the transducers differ in center frequency by a factor of at least about 2.5. In one embodiment, the factor is between about 2.5 and 3. In one specific and non-limiting example, one transducer may have a center frequency of 15 MHz, and the other transducer may have a center frequency greater than about 40 MHz.

[0066] Imaging transducer 105 generally consists of a piezoelectric material 319, commonly PZT-5H, but may include other piezoelectric ceramics, a composite design, a single crystal design, lithium niobate, PVDF and a variety of other materials known for ultrasound transducer fabrication, including cMUT and pMUT transducers. The piezoelectric is coated on both sides 318 and 320 with conductive layers, such as thin layers of gold or other materials with high conductivity. On one side of the piezoelectric layer 319, a backing layer 321 may be applied to dampen undesired acoustic signals from going through the back of the transducer. The backing layer 321 may be electrically conductive, as this simplifies an electrical connection with angle detection transducer 100, as will become apparent below. In an alternative embodiment in which the entire backing layer 321 and/or backing layer 310 is not electrically conductive, suitable electrically connections between signal wire 301, conductive layer 320, and conductive layer 311, may be provided through a conductive channel formed within backing layer 321 and/or backing layer 310 or through a conductive wire connecting the conductive regions. The signal conduction wire 301 is connected electrically to conductive layer 320, such as through a conductive backing layer 321. Alternatively, other conductive paths between signal conduction wire 301 and conductive layer 320 can be used. In the example embodiment of Figure 5a, all regions sharing the electrical connection to the signal conduction wire 301 are labeled with a "+" symbol. At one end of the transducer backing layer 321, an electrically insulating barrier 331 is bonded to the transducer. On the face of the piezoelectric material 318 opposite the backing layer 321, a thin layer of an electrically conductive acoustic impedance matching material 317 is bonded.

[0067] A thin and electrically conductive layer 316 is bonded adjacent to the electrically insulated barrier 331. Ground connection 300 is connected electrically to this layer. All regions sharing the electrical connection to the ground conduction wire 300 are labeled as "GND". The acoustic beam emitted from the imaging transducer is directed along an axis normal to the transducer surface 392.

[0068] Similar to the design of the imaging transducer 105, angle detection transducer 100 consists of a piezoelectric material 312, commonly PZT-5H, but may often include a composite design, a single crystal, lithium niobate, or PVDF and a variety of other materials known in the art. Piezoelectric layer 312 is coated on both sides 311 and 313 with a thin conductive layer, commonly gold. On one side of piezoelectric layer 312, a backing layer 310 is applied to damp out undesired acoustic signals

from going through the back of the transducer. Backing layer 310 may be electrically conductive and electrically connected to backing layer 321. At one end of the transducer backing complex, a thin electrically insulated barrier 330 is bonded to the transducer. On the face of the piezoelectric material 312 opposite backing layer 310, a thin layer of an electrically conductive acoustic impedance matching material 314 is bonded. A thin electrically conductive layer 315 is bonded adjacent to the electrically insulated barrier 330. The acoustic beam emitted

from angle detecting transducer 100 is directed along an axis normal to the transducer surface 394. Alternatively, backing layer 310 may be omitted and conductive layer 311 may be directly bonded to backing layer 321. In this case, the two transducers may share backing layer 321 for damping out unwanted acoustic signals.

[0069] In order for the transducers to share electrical connections in an embodiment in which the transducers form a unitary structure, they may be mounted or bonded such that the conductive ground channels 315 and 316 of each transducer are in direct electrical contact, the electrically insulating barriers 330 and 331 are in continuity, and the backing layers 310 and 321 of both transducers are electrically conductive and in direct contact with each other. There should be high electrical resistance between the electrically conductive signal regions and ground regions of either transducer in order to maintain appropriate connections.

[0070] It is to be understood that the embodiment described in Figure 5a is example of one of several embodiments wherein two ultrasound transducers can share a single electrical channel and form a unitary structure. In an alternative embodiment, one or more of the backing layers need not be electrically conductive, provided that conductive pathways to opposing sides of piezoelectric elements 312 and 319 for each of the transducers are provided. Electrically conductive pathways can be made using materials such as wires, metals, conductive epoxies and other materials known in the art. The pathways may be made using processes such as, but not limited to, layering, bonding, and soldering, sputtering, wire bonding.

[0071] Acoustic matching layers 314 and 317 may improve the efficiency of acousto-electric coupling but may not be necessary for one or more of the transducers. In an alternative embodiment, a plurality of matching layers may be used for one or more of the transducers. Furthermore, electrically insulating barriers 330 and 331 provide example embodiments for electrically isolating the signal and ground pathways from each other but may take on more complex arrangements than described in Figure 5a, and may include a void or gap made of an insulating gas or liquid rather than a solid material. Furthermore, the signal and ground designations of each side of the two transducers are arbitrary and can be connected in several permutations of arrangements.

[0072] Figure 5b illustrates an embodiment for sharing a single electrical connection between the angle detec-

tion transducer 100 and imaging transducer 105 while the two transducers do not form a unitary structure. For example, the transducers may be fabricated in the same way as described in reference to Figure 5a, but are not bonded together. Instead, the signal connection 301 and ground connection 300 from coaxial cable 302 are connected electrically to opposing sides of the piezoelectric elements 313 and 319 both the angle detection transducer 100 and the imaging transducer 105. In the example shown in Figure 5b, all regions sharing the electrical connection to the signal conduction wire 301 are labeled with a "+" symbol. Similarly, the ground connection 300 is connected electrically to both the conductive path 315 on the angle detection transducer 100 and the conductive path 316 on the imaging transducer 105. All regions sharing the electrical connection to the ground conduction wire 300 are labeled as "GND" in Figure 5b. In one example embodiment, the ultrasound transducers operate at substantially different center frequencies.

[0073] In some embodiments, a multi-transducer imaging probe is provided in which the imaging probe houses two or more ultrasonic imaging transducers that are connected to a common electrical channel. Each transducer may be selected to exhibit a unique spectral response that is substantially spectrally distinct and non-overlapping from the other ultrasonic transducers. As noted above, additional electrical filtering may be employed to provide additional spectral isolation among the ultrasonic transducers.

[0074] The imaging transducers may be positioned to direct each ultrasonic imaging beam in a distinct direction, thereby enabling simultaneous imaging at multiple angles. Unlike phased array imaging, in which multiple ultrasonic transducers are driven in a phased relationship by unique and individual electrical channels, the present embodiment enables multi-transducer, multi-angle and/or multi-frequency imaging based using a single electrical channel upon which the signals for exciting the different transducers are multiplexed.

[0075] In one example embodiment, two or more imaging transducers may be oriented to direct their ultrasonic imaging beams in a substantially common direction, which may be useful, for example, for simultaneous imaging in multiple acoustic spectral windows. In other embodiments, as shown below, three or more transducers can be used to form unitary structures similar to those shown in figures 5c and 5d, and that multiple transducers can be oriented at arbitrary angles with respect to each other.

[0076] Figures 5c and 5d show two example embodiments in which an imaging probe houses two imaging transducers oriented with a relative angle of 180° and 90°, respectively. Transducers 399 and 397 are electrically connected via common coaxial conductor 302 (comprising common ground wire 300 and common signal wire 301), and are shown as housed within sheath 43. Connections to the suitable conductive layers of transducers 397 and 399 may be made, for example, as shown

in Figure 5a. It should be noted that conductive paths within the unitary structure can be configured such that conductive paths 300 to 301 connect to a common side of the unitary structure, or in various other arrangements such that the electrical connections within the unitary structure provide appropriate conductive paths to transducers 397 and 399. In other example implementations, the connections to the conductive layers of the transducers may be made, as described above, using materials such as wires, metals, conductive epoxies and other materials known in the art, and pathways may be made using processes such as, but not limited to, layering, bonding, soldering, sputtering, wire bonding.

[0077] Figure 5c demonstrates a catheter housed in a sheath 43 configured for side-viewing imaging with a unitary structure formed by joining ultrasound transducers 397 and 399. Here, transducers 397 and 399 transmit anti-collinear beams, 393 and 395 respectively, in a generally side viewing direction relative to the longitudinal axis of the catheter. Upon a complete revolution of the distal imaging assembly, both transducers will have imaged the same region in tissue. This arrangement may be useful in a situation where it is desired to image the same region of tissue with two different frequencies, often a low frequency for deep penetration and a higher frequency to achieve high resolution. While this embodiment shows beams 393 and 395 being anti-collinear, other useful embodiments would include beams that are anti-parallel, but not necessarily anti-collinear.

[0078] Similarly, Figure 5d shows an example implementation in which ultrasound imaging transducers 397 and 399 are both in a generally side viewing direction while transmitting substantially orthogonally directed beams with the centers of the transducer apertures positioned at approximately the same position along the probe's longitudinal axis. Upon a complete revolution of the distal imaging assembly, both transducers will have imaged the same region in tissue.

[0079] Figures 5c and 5d provide two non-limiting embodiments of imaging probes housing dual transducers that are electrically addressable via a common electrical channel, for which many other related embodiments and design variations are possible. For example, any of the embodiments of the present disclosure involving tiltable, pivotable, rotatable and movable elements for directing an emitted imaging beam may be adapted to further include a second imaging transducer according to the present embodiment, where the second imaging transducer need not necessarily be physically contacted with the first imaging transducer.

[0080] In some embodiments, the second imaging transducer may be positioned or oriented to have a field of view remote from the first imaging transducer. Alternatively, the first and second imaging transducers may have fields of view that overlap to create a combined field of view, wherein the signals from one transducer may be used to provide ultrasound data for one portion of the combined field of view and signals from the second trans-

ducer are preferentially used to provide ultrasound data for another portion of the combined field of view. Ultrasound data from each of the one or more transducers may be used for any of several purposes, including imaging, tissue characterization, sensing of instruments outside the imaging probe, and sensing movement of components within the image probe.

[0081] For example, in the embodiments shown in figures 5c and 5d, a transducer with a first center frequency may be used for imaging more distant regions in the combined field of view, while a second transducer with a lower center frequency than the first transducer may be used for providing higher resolution imaging data in regions closer to the imaging catheter. Furthermore, such embodiments may optionally include one or more angle sensing ultrasonic transducers for detecting the direction of an ultrasonic imaging beam emitted by the first and/or second imaging transducers, where the angle sensing transducers are also connected to the common electrical channel.

[0082] Figure 5e shows a scenario where one imaging transducer 387 is shaped such that it contains features that allow for the mounting of a second transducer 397 at an oblique angle relative to the longitudinal axis of the imaging probe. When the distal imaging assembly is rotated, transducer 387 will image a largely side-viewing region of tissue, while transducer 397 will image a partially forward viewing conical region of tissue.

[0083] Figure 5f shows a configuration of a unitary structure of multiple ultrasound transducers driven on a single channel suitable for situations where multiple collinear imaging beams are desired. In the embodiment shown in the Figure, a lower-frequency beam 389 is transmitted from transducer 391 in parallel with a higher-frequency beam 392 from transducer 397. Transducer 397 also receives corresponding echoes.

[0084] The embodiment shown in Figure 5f may be employed for second order ultrasound field (SURF) imaging. SURF imaging uses acoustic energy in two distinct frequency bands transmitted simultaneously. The energy in one frequency band is generally at a low frequency (a center frequency in the range of 0.5-10MHz) and is used as a modulation or manipulation pulse. The energy in the high frequency band tends to be centered approximately 7-10 times higher than the center frequency of the low frequency band. The high frequency energy band is employed to image the tissue under different modulation pressures, as generated but the modulation or manipulation pulse. Accordingly, referring to Figure 5f, ultrasound transducer 397 may be employed to provide a high frequency imaging beam, while larger ultrasound transducer 391 may be provided to generate a SURF ultrasound beam that is parallel and substantially collinear to the imaging beam. While this technique has been performed with two separate ultrasound transducers with two separate electrical channels, the present embodiment may be performed to achieve SURF imaging with a single electrical channel.

[0085] It may also be desirable to include more than two imaging transducers on the same unitary structure connected by a single electrical channel. Figure 5g shows a configuration including three ultrasound transducers, each of which is characterized by a different center frequency. An example of an application for such an embodiment is again for SURF imaging. A low frequency manipulating beam 389 is transmitted from transducer 391 and used to modulate tissue being imaged, while a higher frequency imaging beam 392 is emitted from transducer 397 in a direction that is collinear to modulating beam 389. Positioned to create an antiparallel, and, in some embodiment, anti-collinear, beam 381 is another transducer 399. The frequency of beam 381 may be selected to be higher than that of imaging beam 392 to provide high resolution imaging. One example of a suitable set of frequencies is a 3MHz modulating beam 389, a 25MHz SURF imaging beam 392, and a 60MHz high frequency imaging beam 381.

[0086] It may also be desirable to combine multi-frequency transducers with other imaging modalities. One potential family of modalities is fiber compatible optical imaging modalities. These may include optical coherence tomography, fluorescence imaging, photoacoustic imaging, angioscopy, Raman spectroscopy and other optical modalities known in the art. Figure 5h shows one such configuration including a unitary structure having three components: (1) an ultrasound transducer 399 having a first center frequency, (2) a second ultrasound transducer 397 having a second center frequency that is different from the first center frequency, with both ultrasonic transducers connected to a common electrical channel, and (3) an optical imaging system 383 configured to generate optical imaging beam 385. In the example embodiment shown in the Figure, the second ultrasound transducer 397 contains a hole and an optical beam director to allow optical imaging beam 385 to emerge substantially collinear with second ultrasound imaging beam 395.

[0087] While the imaging transducers shown in Figure 5 are shown as flat transducers, one or more of them may be curved to provide beam focusing. In many applications, it may be beneficial to provide a focused ultrasound beam, or beams, for improved lateral resolution at a desired depth. It may specifically be desirable to focus higher frequency ultrasound beams at regions of interest that are closer to the imaging assembly, and to focus lower frequency ultrasound beams at regions of interest further from the imaging assembly. This enables lateral resolution high resolution images at multiple depths, giving an effectively improved depth of field. In this case, the highest lateral resolution would be achieved close to the imaging probe, where it is often desired for a number of imaging or image guided procedures such as crossing CTOs, vulnerable plaque detection, or transseptal puncture. An embodiment showing focused transducers is shown in Figure 5i, where a first, low frequency transducer 373 is curved to focus at a depth 375 with acoustic beam 374. A second, high fre-

quency transducer 376 has its acoustic beam 377 focused to a depth 378, which is closer to the imaging probe than 375. There are multiple ways of achieving focus on an ultrasound transducer, including using acoustic lenses, mechanical pressing, machining of a curved surface, or using a flexible piezoelectric such as PVDF or a composite material that can be formed into a curved surface.

[0088] As noted above, in some example embodiments, excitation pulses and detected signals are respectively transmitted to and received from both transducers on a common electrical channel, while enabling the detected signals from each transducer to be separated or demultiplexed for image processing and/or angle determination. There are numerous techniques that can achieve this without departing from the scope of the present embodiment. Selected techniques involve separating the frequency spectra of the imaging signal information and the angle detection signal information.

[0089] One embodiment for demultiplexing both detected signals is illustrated in Figure 6. The center frequencies of both transducers are selected such that there is substantially little or no overlap between the respective transducer spectral bandwidth ranges 396 and 398. If the transducers are adequately separated in terms of frequency spectra, signals from one transducer will not interfere with signals from the other. That is, in the illustrative context of an embodiment involving an imaging transducer 105 and an angle detection transducer 100, an imaging pulse sent to the imaging transducer 105 will not cause a significant acoustic response from the angle detection transducer 100.

[0090] Common definitions of spectral bandwidth in ultrasound are based on the range of frequencies surrounding a peak amplitude of the frequency domain representation of an acoustic or electrical signal generated or detected by an ultrasound transducer. In one embodiment, the spectral bandwidths are at least 6 dB bandwidths. For example, the 6dB spectral bandwidth typically refers to the range of frequencies surrounding a frequency of a peak amplitude in which the amplitude of the signal across that range of frequencies is within 6dB of the peak amplitude. The 20dB and 40 dB spectral bandwidths are also commonly used.

[0091] An example frequency spectrum 396 of imaging transducer 105 and an example frequency spectrum 398 of angle detection transducer 100 are plotted in Figure 6 such that the 6dB points of both transducers intersect with the x-axis. Similarly, an angle detection pulse sent to the angle detection transducer 100 will not cause a significant acoustic response from the imaging transducer 105.

[0092] The frequencies of the two transducers may be selected to avoid harmonics of the transducer center frequencies. In general, it may be advantageous to avoid having the center frequencies of the transducers as integral multiples of one another, so as to avoid confusion caused by harmonics from non-linear echoes. This is especially true for cases where microbubble specific imag-

ing techniques are being used, as many of these techniques rely on harmonics for separation between tissue and contrast agent. The higher frequency transducer may be configured to have a larger absolute bandwidth to take advantage of increased axial resolution at the higher frequency, as shown.

[0093] In some circumstances, imaging excitation pulses may possess a significantly broader bandwidth than that of the imaging transducer, thereby resulting in the possibility of transmitted pulses spectrally overlapping with the bands of both transducers. This may be mitigated using analog or digital filtering techniques to separate the effective bands of the excitation pulses received by the individual transducers.

[0094] In one embodiment, such a filtering scheme may be implemented using passive elements as shown in Figure 7. A filter 380 may be generated from a combination of electrical components, such as resistive, inductive and/or capacitive components, and is employed to spectrally restrict imaging pulses from exciting the angle detection transducer 100, while a filter 390 may be generated from a combination of electrical components to spectrally restrict angle detection pulses from exciting the imaging transducer 105. Alternatively, narrower band excitation pulses can be used for imaging, angle detection or both.

[0095] In another example embodiment, in which both transducers are spectrally isolated as shown in Figure 6, a broadband excitation pulse or waveform may be provided that overlaps the spectral bandwidths of both transducers, or the excitation waveform may include a first spectral component that is within the bandwidth of one transducer, and a second spectral component that is within the bandwidth of another transducer.

[0096] Detected signals are demultiplexed in the frequency domain using spectral filtering techniques to individually resolve the signals detected from each transducer. Spectral filtering of the detected signals may be implemented using either analog or digital filtering, or both. For example, the signal from the single electrical channel can be separated using analog filters to two separate receive channels that may be connected to two separate analog to digital converters in image processing and display system 49. Alternatively, digital spectral filtering can occur on digitally sampled representation of the received signal using a single analog to digital converter where digital processing hardware or software, are used to separate the imaging and angle detection data.

[0097] Figure 8 illustrates an embodiment in which tiltable member 150 is configured to reflect incident radiation from imaging transducer 105, and where the angular deflection of tiltable member 150 is detected using a time of flight method. In this case, imaging transducer 105 is mounted at a fixed location and oriented towards the tiltable member 150.

[0098] As shown in the figure, another imaging transducer or imaging radiation source 103 can be mounted adjacent to, attached to, or transmitting through a hole

bored into the imaging transducer 105 as described in US Patent Publication No. 20080177183. For example, an optical imaging source/receiver 103 could be mounted to ultrasound imaging transducer 105 to provide a second imaging modality within an imaging probe. It is to be understood that it is not necessary that the front surface of reflective tiltable member 150 is the same as the back surface of the reflector 153. The front surface 151 may be constrained to being highly optically and/or acoustically reflective, while it may be desirable for the back surface 153 to be a diffuse acoustic reflector and/or scatterer.

[0099] Figures 8a and 8b illustrate a common embodiment with tiltable member 150 shown at two different tilt angles, where tiltable member 150 is rotatably mounted on pivot axis 152. Angle detection transducer 100 is placed at a fixed location relative to pivot axis 152. Imaging transducer 105 transmits an acoustic beam 120, while optical imaging source 103 transmits an optical beam 130, where both acoustic beam 120 and optical beam 130 are transmitted in a direction towards the front surface 151. Angle detection transducer 100 transmits an acoustic beam 110 towards the back surface 153 of tiltable member 150, and a portion of the beam is reflected back towards the angle detection transducer 100. This may be achieved via diffusive reflection of the incident ultrasonic angle sensing beam.

[0100] In Figure 8a, tiltable member 150 is relatively far from the angle detection transducer 100, along the path of beam 110, when compared to Figure 8b. This results in the angle detection beam 110 having a shorter time of flight in Figure 8b than Figure 8a. The tilt angle can be calculated as described above in reference to Figure 4. Timing diagrams are presented for each angle scenario. A pulse is transmitted at $t=0$ with a high amplitude and received at a later time, typically with a reduced magnitude. Figure 8e shows a sample plot of time delay, or time of flight vs. imaging angle. Figures 8c and 8d are timing diagrams are presented for each angle scenario in Figures 8a and 8b, respectively. The received pulse 502 corresponding to the signal from Figure 8a has a much greater time delay than the received pulse 504 corresponding to the signal from Figure 8b.

[0101] Figures 9a-9e illustrate an embodiment in which the change in angle of a tiltable member, such as ultrasonic imaging transducer 105 is detected using a time of flight method. This embodiment is similar to that of Figure 7, except that ultrasonic imaging transducer 105 is not mounted on a pivoting axis, and is instead mounted on a deformable member 112 whose deformation is responsible for the tilting of the tiltable member.

[0102] Figures 10a-10e illustrates an embodiment in which the change of angle of tiltable member 101 (shown as an imaging transducer) is detected using a signal intensity method. This method is based on the relationship between the intensity of diffusively scattered ultrasonic radiation and the tilt angle, where the reflected signal will be strongest when the angle detection beam 110 is per-

fectly normal to tiltable member 101, as shown in Figure 10a. As the tilt angle changes from normal, the strength of the received signal is reduced (item 504 vs. item 502), as is seen in Figures 10c and 10d. The reduction in received signal intensity or voltage can be used to estimate the tilt angle, as shown in the example calibration curve provided in Figure 10e.

[0103] Figures 10c and 10d are timing diagrams presented for each angle scenario in Figures 10a and 10b, respectively. It is noted that there may be temporal broadening of the signal due reflections coming from different slightly different depths as the imaging transducer 101 is moved away from being normal to the angle detection beam 110. Such an effect is shown in Figure 10d. Accordingly, in selected embodiments, the relative temporal broadening may also be employed to provide feedback relating to the deflection angle. Such an embodiment may be used to confirm and/or improve the accuracy of the deflection angle obtained through intensity measurements.

[0104] In some embodiments, the sensitivity of angle detection may be hindered at large deflection angles due to intensity reduction, as illustrated in Figure 10. The intensity of a received signal from a perfect reflector drops very quickly from angles even slightly off normal from the angle detection beam 110. This makes the signals very difficult to detect, and diffusive reflectors may provide improved performance. There are several potential approaches to overcoming this.

[0105] The difference between a specular and diffusive reflector is illustrated in Figures 11a-d. Figure 11a shows a specular reflective tiltable member 170 receiving an angle detection beam 110 from an angle detection transducer 100. The beam is reflected off the specular reflector 170, and the reflected beam 113 is directed in a path that is not co-incident with the angle detection transducer. The result, as shown in the timing diagram below in Figure 11c, is that the pulse is not received.

[0106] Figure 11b illustrates an embodiment in which the incident beam 110 is reflected by a diffusive reflector. While a portion of the beam 117 may be directed away in a similar fashion as described in Figure 11a, a significant portion of the beam 115 is scattered and diffusively reflected over a wide angular range. A portion of this beam is collinear with the incident beam 110, thus allowing for a time of flight detection technique to be feasible (as shown in Figure 11d by the presence of the reflected pulse).

[0107] Another potential arrangement that can assist with the reduction of signal from a substantially specular reflector is the use of multiple angle detection transducers. Such an embodiment is illustrated in Figures 12a-12d. Here, two angle detection transducers 100, 126 are oriented towards tiltable member 101 which is mounted on pivot axis 102. Each of the angle detection transducers 100, 126 generate their own acoustic beam 110, 127.

[0108] All 3 transducers of the preceding embodiment may be driven by a single electrical channel (for example,

connected to patient interface module 36 of Figure 1). Notably, there will be an overlap in the received signals from the angle detection transducers 100, 126 if they lie within the same frequency range. This can be resolved with prior knowledge of the transducer positions, or by limiting the range of angles through which the tiltable member is allowed to tilt.

[0109] The distance calculated by the time of flight difference between the two received pulses may provide tilt angle information in this case. For instance, if the two angle detection transducers 100, 126 are placed 90° from each other with one of the beams parallel to the longitudinal axis, equidistant from pivot axis 102 and on opposing sides of pivot axis 102 but the same side of tiltable member 101 with a flat surface (as they are in Figure 12), the difference in the time between the received pulses from both transducers will be at a minimum when the tilt angle is 45° from the longitudinal axis (As suggested by Figures 12c and 12d). As the tilt angle moves away from 45°, the time between the received signals between the two transducers will increase, as shown in Figure 12d with received pulses 510, 512 from angle detection transducers 100, 126 respectively.

[0110] Angle sensing transducers 100 and 126 may be selected to have substantially non-overlapping spectral bandwidths, thus allowing the individual detected signals to be separated based on their frequency domain content. Alternatively, one of the angle sensing transducers may be placed further away from tiltable member 101 than the other, thus ensuring that the time delays from each of the angle sensing transducers is distinct from the time delay detected by the other angle sensing transducer.

[0111] Alternatively, knowledge of the expected direction and / or degree of tilt of the tiltable member can be used to algorithmically determine which portions of the sensed signal along the single electrical channel correspond to each of the two or more angle sensing transducers. For example, in the example implementation of an imaging probe having a movable member with an angular orientation that is dependent on the rotational speed of a rotational conduit housed within the imaging probe, if the rotational speed of imaging assembly 50 along the longitudinal axis of imaging probe 44 is increased, it may be expected that the tiltable member would tilt in a more forward looking direction. Therefore, knowledge of the expected direction of tilt could be used to identify which of the peaks in the received signal corresponds to one of the several angle sensing transducers. Similarly, knowledge of the instantaneous rotational velocity of the imaging assembly may correspond with a greater likelihood to a particular range of tilt angles, and such a relationship could be used to identify which of the peaks of the received signal most likely corresponds to one of the several angle sensing transducers.

[0112] Figures 13a-13e illustrates an embodiment that enables sensitive angular detection while increasing the range of angles that can be detected by the angle detec-

tion transducer 100. In this embodiment, the back surface of tiltable member 183 (which may also include an imaging transducer, as shown in Figure 13) has been shaped with a series of curved indentations. As the transmitted beam 110 hits the back of tiltable member 183, a small portion of the reflective interface will be substantially normal to the incident beam 110, causing part of the beam 181 to be reflected back to angle detection transducer 100. Accordingly, the angle can be resolved using a time of flight method similar to Figure 4. It is to be understood that the specific cylindrical surface patterning illustrated in Figure 13 is merely one non-limiting embodiment, and that a wide range of surface profiles may be employed to achieve a similar result according to the present embodiment. For example, parabolic cross-sections, or a pattern of divots may be used on the back surface of tiltable member 183.

[0113] While the preceding embodiments have disclosed surfaces that are diffusively reflective, it is to be understood that diffusive reflections may be generated by surface and/or volume material properties. For example, particles of metals, ceramics, silicon dioxide, graphite, glass beads, or other compounds known in the art can be added to a material or surface to make it more diffusely reflective.

[0114] The use of composite materials or flexible polymers has allowed for ultrasound imaging transducers to be shaped physically. Such transducers may be employed for focusing acoustic energy. Alternatively, acoustic lenses may also be used to focus acoustic energy. However, such schemes may be adapted to the present embodiments to broaden the acoustic beam and support an increase in the range of angles that can be detected. This is illustrated in Figures 14a-14d, where angle detection transducer 200 is curved such that it creates diverging beam 210. As shown in the Figure, a portion of the beam is normal to the imaging transducer 101 at a wide range of angles. The normal portion of the beam 220 is reflected back to the transducer, even when the tiltable member is a specular reflector, and may be measured to estimate tilt angle using a time of flight method as in Figure 4.

[0115] Yet another embodiment for increasing the range of angles that can be detected may be achieved by attaching the angle detection transducer to the tiltable member. Figures 15a-15e shows an example of one such embodiment. In this embodiment, angle detection transducer 100 is mounted to the back of the tiltable member 101. The angle detection beam 110 is directed towards stationary reflector 174. A portion of stationary reflector 174 may be curved (in any of several shapes) to provide a suitable angle-dependent acoustic reflection profile. Example yet non-limiting curvature profiles include circular, elliptical or parabolic shapes.

[0116] In one embodiment, the stationary reflector 174 may be shaped so that over a wide range of imaging transducer 101 tilt angles, the reflection from the angle detection beam 110 is largely retro-reflected towards the

angle detection transducer 100. As shown in Figures 15c and 15d, one or both of the time of flight and intensity schemes may be employed to infer changes in the orientation of tiltable member 101.

[0117] Figure 15e describes one method to design a stationary retroreflecting acoustic reflector. The angle detection transducer 100 is modeled in a forward viewing position, as defined by tilt axis 600. A desired distance 608 between angle detection transducer 100 and the reflecting surface is chosen and a data point is generated on a line normal to transducer 100 a distance 608 away from transducer 100. The angle detection transducer is tilted by angle 616 about pivot point 102 and desired distance 610 between angle detection transducer and reflecting is chosen to differ from 608 by a selected amount, such as an amount for obtaining a desired angular resolution. A data point is generated as with the above. This process is repeated until the angle detection transducer is tilted to the point that it is side viewing. A continuous surface 601 is defined by interpolating the data points generated as described above using known curve fitting techniques. Examples of suitable curves that can be fitted are portions of an ellipse, parabola, circle, hyperbola, exponential, roulette, or polynomial using fitting strategies common in the art including but not limited to ordinary least squares or total least squares.

[0118] Once a surface is defined and fabricated, there may be imperfections in machining tolerances and misalignments in assembly among other uncertainties. In order to mitigate this, calibration of an angle detection assembly may be used to overcome these imperfections.

[0119] According to another embodiment, the surface 601 is defined such that the angle detection beam emitted by the angle sensing ultrasonic transducer 100 is substantially retroreflected over a given range of pivot angles, such that the distance between surface 601 and angle sensing ultrasonic transducer 100 varies monotonically over the range of pivot angles, and such that the rate of change of the relative distance with respect to the pivot angle (which, at least in part, determines the resolution of the apparatus), exceeds a minimum value over the range of pivot angles. In one embodiment, surface 601 is configured such that the rate of change of the relative distance with respect to the pivot angle is substantially constant over the range of pivot angles, such that the sensitivity of the apparatus is substantially independent of pivot angle over the range of pivot angles.

[0120] As noted above, in some embodiments, the angle of the detection beam may be constrained to remain approximately normal to the reflective surface of the tiltable member, thereby generating a retroreflection. This eliminates the need to compensate for reflections at angles where the angle detection beam is not normal to the tiltable member, and generally results in detected beam of higher intensity. Example embodiments utilizing such an approach are shown in Figures 16 and 17. Figures 16 a-d illustrate an embodiment in which angle detection transducer 100 is mounted onto second tiltable member

114 that is mechanically linked or coupled to first tiltable member 101 via coupling mechanism 176. Secondary tiltable member 114 is not necessarily acoustically active (and may be acoustically passive) and allowed to pivot about axis 104.

[0121] Since both members are able to pivot about their own pivot axes and are mechanically coupled, they will tilt in unison. The tiltable members are mechanically coupled such that they tilt with a substantially equal tilt angle during operation. A number of techniques may also be used to couple the motion of the tiltable members, including, but not limited to, rods, beams, magnets, and electromagnetic devices. The embodiments shown in Figures 16 and 17 have the additional benefit of adding another tiltable member to the system that may not suffer from inertial or other design constraints of the first tiltable member, such as being an ultrasound transducer optimized for acoustic performance.

[0122] Such a scheme may be useful in cases where first tiltable member includes an ultrasonic imaging transducer, but does not possess suitable characteristics for external rotational actuation. By incorporating secondary tiltable member 114 with characteristics designed for actuation via external rotation and mechanically linking both tiltable members, first tiltable member 101 can be actuated based on the behavior of second tiltable member 114. For example, as shown in Figures 4f and 4g, ultrasound transducers may have similar or larger dimensions in the range direction compared to the elevation directions. This is largely due to the requirement for backing on an ultrasound transducer to attenuate signals in directions other than the desired imaging direction. Bodies of this geometric configuration are not ideal for actuation via external rotation, as shown in Figures 4f and 4g.

[0123] Figure 4f shows a body 134 that has a similar dimension in the range direction relative to the elevation direction. Here, the body pivots about point 137 under rotation in direction 63. If the body is broken into two components, one above longitudinal axis 131 and one below, the center of mass of the components above and below longitudinal axis 131 are shown at 136 and 133 respectively. The centripetal force vectors are shown as 135 and 132 respectively.

[0124] Now, comparing to a body shown in Figure 4g, where the dimension in the range direction is much smaller than the dimension in the elevation direction, we see similarly that the body pivots about point 121 under rotation in direction 63. If the body is broken into two components, one above longitudinal axis 122 and one below, the center of mass of the components above and below longitudinal axis 122 are shown at 124 and 128 respectively. The centripetal force vectors are shown as 129 and 123 respectively. The result is that the pivotally mounted body 125 in Figure 4g has a much stronger relative component of centripetal force that acts to cause tilt about the pivot point 121 than body 134 does about pivot point 137.

[0125] This mechanical coupling may also allow angle

detection beam 110 to remain normal to the ultrasound imaging transducer 101. Other techniques that additional deflectable member can employ to assist in deflection may include the use of hydrofoil features or artificial muscle actuation.

[0126] A time of flight technique can be used to estimate the imaging angle, similar to that shown in Figure 4. Alternatively, or additionally, an intensity measurement method may be employed, as illustrated in Figures 10c and 10d.

[0127] Figure 16e illustrates some of the parameters that may be employed to calculate the tilt angle θ based on measured distance 400. If the distance 401 between acoustically passive disc 114 and the imaging transducer 101 is constant and known a priori, and the distance between the angle detection transducer 100 and the imaging transducer 101 is determined with the knowledge of the signal time of flight and the speed of sound in the medium, the angle can be calculated with the trigonometric equation $\theta = \text{arcCos}(\text{measured_distance } 400 / \text{known distance } 401)$.

[0128] In a similar embodiment, illustrated in Figures 17a-17d, angle detection transducer 100 can be mounted on the tiltable member 101, and maintained in a normal orientation relative to acoustically passive tiltable member 114. A unitary structure similar to that shown in Figure 5a would be suitable for use as the tiltable member 101 in Figure 17a.

[0129] Figure 18a illustrates an embodiment that combines the features shown in Figures 15 and 17. Here, the stationary curved reflector 174 is employed to increase the range of angles that can be detected using the angle detection transducer 100. This is achieved by separating the imaging transducer 101 and the acoustically passive tiltable member 114 in space sufficiently such that they do not come into contact with each other regardless of tilt angle (within the range permitted during operation), while still allowing the acoustically passive second tiltable member 114 to be employed to assist the ultrasound imaging transducer 101 in achieving desired motion using mechanical coupler 176.

[0130] Figure 18b shows a view cut of an example embodiment through the hatched line in Figure 18a. A notch 177 in the stationary curved reflector 174 is created such that the mechanical coupler 176 is allowed to pass through the stationary reflector 174 unimpeded. By way of example, mechanical coupler 176 may include a simple bar or rod that is connected to each of the tiltable members 114 and 101 by a hinge or other mechanism, such as a mechanism that creates a pivot point or deformable joint between mechanical coupler 176 and each of the tiltable members.

[0131] Figures 18 c-i demonstrate another apparatus for detecting tilt angle where the angle detection transducer 100 is mounted inside the notch 177 of supporting structure 175 instead of being attached to the tiltable member 101. Figures 18c and 18e show the setup at two different tilt angles. Cut view through the hatched lines

in Figure 18c and 18e are shown in Figures 18d and 18f respectively. Figures 18g and 18h show the timing diagrams for Figures 18d and 18f respectively. In Figure 18d, the mechanical coupling bar 176 is near the top of the notch 177 resulting in the received signal in 18g having a long delay, whereas in Figure 18f it is considerably further down within the notch, and is subsequently closer to the angle detection transducer resulting in a received signal with a shorter time delay. Figure 18i shows a plot estimating deflection angle vs. time delay. Alternatively, the angle detection transducer 100 can be mounted on mechanical coupling bar 176 and pointed towards the bottom of notch 177.

[0132] Figures 18c-i show how a second transducer 100 can be used to detect the position of a component within an imaging probe. While the position information may be used to infer the tilt angle of a tiltable component, the ability to more generally gather information about the position of a movable component within an imaging probe by using a second transducer that shares a common single channel with another ultrasound transducer becomes apparent.

[0133] Although Figure 18 provides one example embodiment in which an additional ultrasonic transducer is employed for detecting changes in a position of a movable component, it is to be understood that this embodiment may be employed in a wide number of applications for detecting motion of a component within an ultrasonic probe. Other illustrative examples in which the motion of a component may be detected include features in the sheath during a pullback operation, a retractable sheath, the presence of bubbles, a change in fluid density in the catheter, or a therapeutic tool such as a Brockenborough needle.

[0134] Accordingly, it is to be understood that the scope of the embodiments disclosed herein is not to be limited to those in which an angular orientation or a change in an angular orientation of a movable component is determined using one or more additional ultrasonic transducers, and further encompasses embodiments in which a position or a change in position of a movable component is determined using one or more additional ultrasonic transducers, irrespective of whether or not the position or change in position relates to an angular orientation or a change in angular orientation.

[0135] Figure 19 shows an example time-domain imaging and angular detection sequence for a single pulse-echo ultrasound imaging sequence using the embodiment described in Figure 17. In Figure 19a, imaging transducer 101 is excited with a low frequency pulse, as shown in the timing diagram shown in Figure 19b. The pulse generates an acoustic beam 120 which propagates until it reaches an object 106 in its path. Part of the beam is reflected, and detected by the imaging transducer, and as a result displayed in the "Receive" portion of the timing diagram. Next, the residual beam meets another object 108, and again, a part of the beam is reflected, and detected by the imaging transducer and likewise appears

as a received signal, slightly further along the "Receive" timing diagram.

[0136] After imaging data is received, a high frequency angle detection pulse is transmitted down the same channel, generating an acoustic beam 110 from the angle detection transducer 100. This beam is reflected off the acoustically passive member 114 and returned to the transducer. The tilt angle is determined using the time of flight of the beam 110 following the high frequency pulse generation.

[0137] As described above, this embodiment can be optionally aided with the use of one or more electronic filters to select the desired frequency components. For example, a low pass filter may be used to emphasize low frequency signals from the low frequency imaging transducer 101 following transmission of an imaging pulse 550, while a high pass filter may be used to emphasize the high frequency signals from high frequency angle detection transducer 100 following the transmission of angle detection pulse 500. These filters may reside within the imaging probe, or optionally external to the imaging probe, such as within controller and processing unit 34 or patient interface module 36.

[0138] Figure 19c-e shows an embodiment where both transducers are excited with a broadband pulse that covers the bandwidths of both imaging transducer 101 and angle detection transducer 100. The received signal from both transducers is demultiplexed in order to separately process the imaging signal data and the angle sensing data. Such demultiplexing may be achieved according to one of many embodiments.

[0139] In one such discriminatory embodiment, as described in Figure 19d, a time domain method is employed utilizing the fact that there may be a significant difference in the distance between a) the angle detection transducer 100 and the second deflectable member 114 and b) the imaging transducer 101 and the acoustic imaging targets 106 and 108. The distance between the angle detection transducer 100 and the second deflectable member 114 may be significantly less than the distance between the imaging transducer 101 and the acoustic imaging targets 106 and 108. In this arrangement, signals received 558 shortly after transmission 560 pulse is sent may be deemed to be as a result of the angle detecting transducer 100, and signals received after later time delays 554, 556 may be deemed to be as a result of the imaging transducer 101. Accordingly, in such an embodiment, all pulses received prior to the vertical hatched line 562 are deemed to be angle detection pulses and those received after are deemed to be imaging pulses.

[0140] A second embodiment for demultiplexing the signals may be achieved by spectrally filtering or separating the spectral content contained within the net signal and can be achieved using the same embodiment shown in Figure 19c. A representative timing diagram is shown in Figure 19d as described above. Since the bandwidths of the transducers are sufficiently separated and may be known, signals falling within the bandwidth of the angle

detection transducer 100 can be deemed to be originating from the angle detection transducer 100, and signals falling within the bandwidth of the imaging transducer can be deemed to be originating from the imaging transducer.

[0141] This spectral separation is shown the spectral plot in Figure 19e, where the vertical hatched line 564 is used to show a point representing the separation between imaging data and angle detection data. This line 5 may be the midpoint between the center frequencies of the two transducers. All spectral components lower than the frequency represented by the hatched line are deemed to be components of the imaging signal 568, and all spectral components higher than the frequency 10 represented by the hatched line are deemed to be components of the angle detection signal. Also, the separation 15 may be defined more than a single line. For instance, the -6dB, -20dB or -40 dB bandwidths may be used as points to separate data between angle detection and imaging. Furthermore, the both the time of flight demultiplexing and spectral demultiplexing techniques 20 described for Figure 19c-e above can be combined.

[0142] It is to be understood that there are many methods 25 that can be employed to obtain sufficient spectral isolation of the two signals. As described above, filtering techniques may be employed to separate the spectral signals received from each transducer. In another embodiment, spectral windows corresponding to each transducer may be determined based on an isolation criteria. For example, the upper end of the spectral window 30 for the lower-frequency transducer may be selected as corresponding to the point at which the spectral response of the higher-frequency transducer falls below a desired value (for example, 20 dB).

[0143] In some situations, it may be desirable to excite the ultrasound transducers at different points in time, with differing repetition frequencies. One example of this is where one of the transducers is configured for angle detection. In this scenario, changes in angle may be extremely minute such that it may be unnecessary to perform angle detection with at the pulse repetition rate required for imaging. For example, it may be that the angle is expected to remain relatively constant over the amount of time required to acquire multiple imaging vectors. A 45 pulse sequence can be defined such that imaging pulses 550 are transmitted and acquired much more frequently than angle detection pulses 500, as shown in Figure 19f.

[0144] Similarly, it may be desirable in some situations to allow more time for echo return from one ultrasound 50 transducer than the other. One example of this is where one of the transducers is configured for angle detection. In this scenario, it is often the case that the transducer configured for angle detection is of higher frequency than the transducer configured for imaging. Furthermore, it is often the case that the angle detection is performed using echoes from locations that are spatially very close to the angle detection transducer, requiring relatively little acquisition time to ensure capture of echoes associated 55

with angle detection.

[0145] This scenario is illustrated in Figure 19g. Imaging pulse 550 is transmitted and a relatively long period of time 420 is dedicated to waiting for echoes associated with imaging pulse 550. Conversely, relatively little time 422 is dedicated to waiting for echoes associated with angle detection pulse 500.

[0146] In some embodiments, the temporal spacing between imaging pulses may be configured to be variable. By way of example, in situations where a motor encoder is used as a trigger for imaging pulses, the imaging pulse repetition frequency will be higher the motor is rotating more quickly than when the motor is rotating more slowly. Accordingly, the pulse repetition frequency for angle detection may also be selected to be variable, and to be determined by the pulse repetition frequency of imaging.

[0147] It is to be understood that Figures 4, and 8 through 19 represent embodiments that are typically housed within the imaging assembly 50, but that the other components of the imaging assembly are not shown for simplicity.

[0148] Figure 20 illustrates three different techniques for calculating the relative distance travelled by the ultrasonic angle sensing beam, based on the detected radio-frequency (RF) signals. The first method, shown in Figure 20a, involves calculating the peak value of the RF signal for each pulse. As shown, the received electronic pulse includes a pulse envelope and oscillations of a carrier wave. The first pulse 402 is shown as arriving relatively early compared to the second pulse 404. This implies that the angle detection transducer 100 is closer to the tiltable member 101, with the first pulse 402 (for example, as shown in Figure 4b) than the second pulse 404 (for example, as shown in Figure 4a). The difference 414 between the peak RF value 406 from the first signal and the second signal 408 can be used to estimate the distance between the two points which can then be used to infer the tilt angle.

[0149] However, the RF signal in the carrier wave can fluctuate significantly as a result of minor changes in sub-resolution scatterers, and it follows that using the RF peak detection method can lead to inaccuracies when measuring small changes in position. For example, if a new peak emerges, there will be significant error in the measurement of distance between the angle detection transducer and the imaging transducer.

[0150] Another approach is to first calculate the envelopes of signals (407 and 409 for RF signals 402 and 404 respectively) and using the difference 416 between the envelope peaks (410 and 411 for envelopes 407 and 409 respectively) to estimate distance. Some of the fluctuation issues described with using the RF peak method are eliminated with this technique.

[0151] Another example employs the cross correlation between two signals to estimate the distance between subsequent received RF pulses. An example embodiment is shown in Figure 20b. The cross correlation be-

tween the first 402 and second 404 RF pulses is shown as 413, with the peak of the cross correlation signal being detected as 412. The amount of time between time 0 and the peak value is given as 418 and can be used to calculate the distance travelled between two tilt angles to calculate angular shift.

[0152] Generally, the cross-correlation may be performed between a given pulse and another recorded pulse, such as a previously recorded pulse obtained at a different angular tilt. Alternatively, the cross correlation may be performed between a given pulse and a pulse stored at time of calibration of the imaging probe and retrieved from the EEPROM or other memory mechanism associated with imaging probe 44. Alternatively, the cross correlation may be performed between a given pulse and a standardized pulse for a particular design of imaging probe 44, assuming that the pulses generated by the angle detecting transducer are adequately reproducible between imaging probes fabricated from the same design.

[0153] In the preceding angle-detection embodiments, outliers may be detected and rejected to improve the performance angle detection. There are several known techniques for rejecting outliers which could be applied including statistical techniques and voting methods. Figure 21 shows experimental measurements of using an angle detection scheme corresponding to the embodiment described in Figure 18a. Distances between two tiltable disc-shaped members were calculated using the cross-correlation method from Figure 20b. The tiltable members were tilted using a microstage that continuously advanced a rod against the surface of one of the tiltable members causing the two tiltable members to tilt in unison. The position of the rod (in microns) is shown on the x-axis. The normal distance measured between the two tiltable members as measured by an angle detecting transducer on one of the tiltable members is shown on the y-axis (in microns), as depicted in Figure 17. The tilt angle subtended by the tiltable members with an arbitrary axis could be calculated at each time point based on the measured distance between the two members. This angle was compared to the expected angle based on a solid model.

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Claims

1. An imaging probe comprising:

50 a longitudinal body (44);
a first ultrasonic transducer (105) provided within said longitudinal body (44), wherein said first ultrasonic transducer (105) is located remote from a proximal end of said longitudinal body (44), and wherein said first ultrasonic transducer (105) is configured to deliver an ultrasonic imaging beam to a region outside of said longitudinal body (44) and to receive reflected ultrason-

ic imaging energy from the region; a second ultrasonic transducer (100) housed within said longitudinal body (44); and electrically conductive paths extending through said longitudinal body (44) and defining a common electrical channel; 5 wherein said first ultrasonic transducer (105) and said second ultrasonic transducer (100) are connected to said common electrical channel, and wherein said common electrical channel is electrically connectable to an image processing system (49); 10 wherein said first ultrasonic transducer (105) and said second ultrasonic transducer (100) each exhibit substantially non-overlapping spectral bandwidths; 15 **characterized in that** said imaging probe further comprises an imaging assembly (50) housed within said longitudinal body (44), wherein said first ultrasonic transducer (105) is provided within said imaging assembly (50); 20 wherein said imaging assembly (50) includes a movable member (101) for scanning an angular orientation of the ultrasonic imaging beam; and wherein said second ultrasonic transducer (100) is an angle sensing ultrasonic transducer (100) configured for generating an angle sensing ultrasonic beam and generating an angle sensing signal associated with an angular orientation of 25 said movable member (101) relative to a longitudinal axis of said longitudinal body (44). 30

2. The imaging probe according to claim 1 wherein said second ultrasonic transducer (100) is mounted to said first ultrasonic transducer (105). 35

3. The imaging probe according to claims 1 or 2 wherein said first ultrasonic transducer (105) is configured to pivot about a pivot axis. 40

4. The imaging probe according to any one of claims 1 to 3 wherein the ultrasonic imaging beam is a first ultrasonic beam, said second ultrasonic transducer (100) is an imaging transducer configured to produce an additional ultrasonic imaging beam. 45

5. The imaging probe according to claim 4 wherein said second ultrasonic transducer (100) is configured to deliver the additional ultrasonic imaging beam in a direction that is substantially anti-collinear to that of the first ultrasonic beam. 50

6. The imaging probe according to claim 1 wherein said imaging assembly (50) further includes an acoustically reflective substrate, wherein said angle sensing ultrasonic transducer (100) is configured to direct an angle sensing ultrasonic beam towards said acoustically reflective substrate and to receive a reflected 55 ultrasonic beam reflected from said acoustically reflective substrate, such that an angle sensing signal produced by said angle sensing ultrasonic transducer (100) in response to the reflected ultrasonic beam is detectable on said common electrical channel, and wherein said acoustically reflective substrate is positioned relative to said movable member (101) such that a change in an orientation of said movable member (101) relative to a longitudinal axis of said longitudinal body (44) produces a change in the angle sensing signal. 7. The imaging probe according to claim 6 wherein said acoustically reflective substrate is configured such that the change in the angle sensing signal includes a relative time delay of the angle sensing signal. 8. The imaging probe according to claim 6 wherein said first ultrasonic transducer (105) and said angle sensing ultrasonic transducer (100) form at least a portion of said movable member (101); wherein said acoustically reflective substrate includes a curved surface profile, wherein a curvature of said curved surface profile is selected such that a deflection of said movable member (101) produces a change in a relative time delay of the angle sensing signal; and wherein said curved surface profile is selected such that a distance between said angle sensing ultrasonic transducer (100) and said acoustically reflective substrate, as determined along a beam path of the angle sensing ultrasonic beam, varies over a defined angular range of said pivotable member. 9. The imaging probe according to claim 6 wherein said movable member (101) includes a first deflectable member (101) mechanically coupled to a second deflectable member (114), such that a change in an orientation of said first deflectable member (101) produces a corresponding change in an orientation of said second deflectable member (114), and wherein a change in the orientation of said second deflectable (114) member produces a change in the direction of the ultrasonic imaging beam. 10. The imaging probe according to claim 6 wherein said angle sensing ultrasonic transducer (100) is positioned such that the angle sensing ultrasonic beam is constrained to be directed approximately normal to a surface of said acoustically reflective substrate. 11. The imaging probe according to any one of claims 6 to 10 further including a delivery and detection subsystem for delivering electrical energy to said first ultrasonic transducer (105) and said angle sensing ultrasonic transducer (100), and for detecting electrical signals detected by said first ultrasonic transducer (105) and said angle sensing ultrasonic trans-

ducer (100).

12. The imaging probe according to claim 11 wherein said first ultrasonic transducer (105) and said angle sensing ultrasonic transducer (100) are each **characterized by** non-overlapping spectral bandwidths, and wherein said delivery and detection subsystem is configured for delivering broadband electrical energy to said first ultrasonic transducer (105) and said angle sensing ultrasonic transducer (100) such that a spectrum of the broadband electrical energy overlaps a spectral bandwidth of said first ultrasonic transducer (105) and said angle sensing ultrasonic transducer (100). 5

13. The imaging probe according to claim 11 wherein said first ultrasonic transducer (105) and said angle sensing ultrasonic transducer (100) are each **characterized by** non-overlapping spectral bandwidths, and wherein said delivery and detection subsystem is configured for delivering electrical energy to said first ultrasonic transducer (105) and said angle sensing ultrasonic transducer (100) such that a spectrum of the electrical energy includes a first spectral component within a spectral bandwidth of said first ultrasonic transducer (105) and a second spectral component within a spectral bandwidth of said angle sensing ultrasonic transducer (100). 10

14. The imaging probe according to claim 12 or 13 wherein said delivery and detection subsystem further includes a processor, wherein said processor is programmed to determine, based on the change in the angle sensing signal, a corresponding change in a direction of the ultrasonic imaging beam. 15

15. The imaging probe according to claim 14 wherein said processor is programmed to control a direction of the ultrasonic imaging beam based on feedback from the angle sensing signal. 20

16. A method of determining a direction of an imaging beam emitted by an imaging probe, the method including the steps of: 25

providing an imaging probe according to any one of claims 6 to 10;

providing one or more electrical pulses to the common electrical channel, wherein the one or more pulses are selected to generate the ultrasonic imaging beam and the angle sensing ultrasonic beam; 30

receiving an electrical signal on the common electrical channel, the electrical signal being generated by the angle sensing ultrasonic transducer (100) in response to the reflected ultrasonic beam and by the imaging ultrasonic transducer in response to the reflected ultrasonic im- 35

aging energy;

demultiplexing the electrical signal and extracting the angle sensing signal; and

relating the angle sensing signal to a direction of the ultrasonic imaging beam. 40

17. The method according to claim 16 wherein the step of relating the angle sensing signal to a direction of the ultrasonic imaging beam is performed by comparing one of an intensity of the angle sensing signal and a time delay of the angle sensing signal to a pre-determined value. 45

15 Patentansprüche

1. Bildgebungssonde, umfassend:

einen Längskörper (44);
 einen ersten Ultraschallwandler (105), der in dem Längskörper (44) bereitgestellt ist, wobei der erste Ultraschallwandler (105) von einem proximalen Ende des Längskörpers (44) entfernt angeordnet ist und der erste Ultraschallwandler (105) konfiguriert ist, einen Ultraschallbildgebungsstrahl an einen Bereich außerhalb des Längskörpers (44) zu liefern und reflektierte Ultraschallbildgebungsenergie aus dem Bereich zu empfangen;
 einen zweiten Ultraschallwandler (100), der in dem Längskörper (44) untergebracht ist; und elektrisch leitende Pfade, die sich durch den Längskörper (44) erstrecken und einen gemeinsamen elektrischen Kanal definieren; wobei der erste Ultraschallwandler (105) und der zweite Ultraschallwandler (100) mit dem gemeinsamen elektrischen Kanal verbunden sind und wobei der gemeinsame elektrische Kanal elektrisch mit einem Bildverarbeitungssystem (49) verbindbar ist;
 wobei der erste Ultraschallwandler (105) und der zweite Ultraschallwandler (100) jeweils im Wesentlichen nicht überlappende Spektralbandbreiten aufweisen;
dadurch gekennzeichnet, dass die Bildgebungssonde ferner eine Bildgebungsanordnung (50) umfasst, die in dem Längskörper (44) untergebracht ist, wobei der erste Ultraschallwandler (105) innerhalb der Bildgebungsanordnung (50) bereitgestellt ist; wobei die Bildgebungsanordnung (50) ein bewegliches Element (101) zum Scannen einer Winkelorientierung des Ultraschallbildgebungsstrahls einschließt; und wobei der zweite Ultraschallwandler (100) ein Winkelabtastultraschallwandler (100) ist, der konfiguriert ist zum Erzeugen eines Winkelabtastultraschallstrahls und zum Erzeugen eines

Winkelabtastsignals, das mit einer Winkelorientierung des beweglichen Elements (101) relativ zu einer Längsachse des Längskörpers (44) assoziiert ist.

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2. Bildgebungssonde nach Anspruch 1, wobei der zweite Ultraschallwandler (100) an dem ersten Ultraschallwandler (105) angebracht ist.

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3. Bildgebungssonde nach Anspruch 1 oder 2, wobei der erste Ultraschallwandler (105) konfiguriert ist, um sich um eine Schwenkachse zu schwenken.

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4. Bildgebungssonde nach einem der Ansprüche 1 bis 3, wobei der Ultraschallbildgebungsstrahl ein erster Ultraschallstrahl ist, und der zweite Ultraschallwandler (100) ein Bildgebungswandler ist, der konfiguriert ist, einen zusätzlichen Ultraschallbildgebungsstrahl zu erzeugen.

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5. Bildgebungssonde nach Anspruch 4, wobei der zweite Ultraschallwandler (100) konfiguriert ist, den zusätzlichen Ultraschallbildgebungsstrahl in eine Richtung zu liefern, die im Wesentlichen antikollinear zu der des ersten Ultraschallstrahls ist.

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6. Bildgebungssonde nach Anspruch 1, wobei die Bildgebungsanordnung (50) ferner ein akustisch reflektierendes Substrat einschließt, wobei der Winkelabtastultraschallwandler (100) konfiguriert ist, einen Winkelabtastultraschallstrahl auf das akustisch reflektierende Substrat zu richten und einen reflektierten Ultraschallstrahl zu empfangen, der von dem akustisch reflektierenden Substrat reflektiert wird, so dass ein Winkelabtastsignal, das von dem Winkelabtastultraschallwandler (100) als Antwort auf den reflektierten Ultraschallstrahl erzeugt wird, auf dem gemeinsamen elektrischen Kanal detektierbar ist, und wobei das akustisch reflektierende Substrat relativ zu dem bewegbaren Element (101) derart positioniert ist, dass eine Änderung in einer Orientierung des beweglichen Elements (101) relativ zu einer Längsachse des Längskörpers (44) eine Änderung in dem Winkelabtastsignal erzeugt.

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7. Bildgebungssonde nach Anspruch 6, wobei das akustisch reflektierende Substrat so konfiguriert ist, dass die Änderung des Winkelabtastsignals eine relative Zeitverzögerung des Winkelabtastsignals einschließt.

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8. Bildgebungssonde nach Anspruch 6, wobei der erste Ultraschallwandler (105) und der Winkelabtastultraschallwandler (100) mindestens einen Abschnitt des beweglichen Elements (101) bilden; wobei das akustisch reflektierende Substrat ein gekrümmtes Oberflächenprofil einschließt, wobei eine Krümmung des gekrümmten Oberflächenprofils so gewählt ist, dass eine Auslenkung des beweglichen Elements (101) eine Änderung in einer relativen Zeitverzögerung des Winkelabtastsignals erzeugt; und wobei das gekrümmte Oberflächenprofil so gewählt ist, dass ein Abstand zwischen dem Winkelabtastultraschallwandler (100) und dem akustisch reflektierenden Substrat, der entlang eines Strahlwegs des Winkelabtastultraschallstrahls bestimmt wird, über einen definierten Winkelbereich des schwenkbaren Elements variiert.

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9. Bildgebungssonde nach Anspruch 6, wobei das bewegliche Element (101) ein erstes auslenkbares Element (101) aufweist, das mechanisch mit einem zweiten auslenkbaren Element (114) gekoppelt ist, so dass eine Änderung in einer Orientierung des ersten auslenkbaren Elements (101) eine entsprechende Änderung in einer Orientierung des zweiten auslenkbaren Elements (114) erzeugt, und wobei eine Änderung in der Orientierung des zweiten auslenkbaren (114) Elements eine Änderung in der Richtung des Ultraschallbildgebungsstrahls erzeugt.

10. Bildgebungssonde nach Anspruch 6, wobei der Winkelabtastultraschallwandler (100) so positioniert ist, dass der Winkelabtastultraschallstrahl so beschränkt ist, dass er etwa senkrecht zu einer Oberfläche des akustisch reflektierenden Substrats gerichtet ist.

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11. Bildgebungssonde nach einem der Ansprüche 6 bis 10, die ferner ein Lieferungs- und Erfassungsunter system zum Liefern elektrischer Energie an den ersten Ultraschallwandler (105) und den Winkelabtastultraschallwandler (100) und zum Erfassen von elektrischen Signalen, die von dem ersten Ultraschallwandler (105) und den Winkelabtastultraschallwandler (100) erfasst werden, einschließt.

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12. Bildgebungssonde nach Anspruch 11, wobei der erste Ultraschallwandler (105) und der Winkelabtastultraschallwandler (100) jeweils durch sich nicht überlappende Spektralbandbreiten gekennzeichnet sind und wobei das Lieferungs- und Erfassungsunter system konfiguriert ist, an den ersten Ultraschallwandler (105) und den Winkelabtastultraschallwandler (100) derart elektrische Breitbandenergie zu liefern, dass ein Spektrum der elektrischen Breitbandenergie eine Spektralbandbreite des ersten Ultraschallwandlers (105) und des Winkelabtastultraschallwandlers (100) überlappt.

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13. Bildgebungssonde nach Anspruch 11, wobei der erste Ultraschallwandler (105) und der Winkelabtastultraschallwandler (100) jeweils durch sich nicht überlappende Spektralbandbreiten gekennzeichnet sind, und wobei das Lieferungs- und Erfassungsunter system konfiguriert ist, an den ersten Ultraschall-

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wandler (105) und den Winkelabtastultraschallwandler (100) derart elektrische Breitbandenergie zu liefern, dass ein Spektrum der elektrischen Energie eine erste Spektralkomponente innerhalb einer Spektralbandbreite des ersten Ultraschallwandlers (105) und eine zweite Spektralkomponente innerhalb einer Spektralbandbreite des Winkelabtastultraschallwandlers (100) einschließt.

14. Bildgebungssonde nach Anspruch 12 oder 13, wobei das Lieferungs- und Erfassungsundersystem ferner einen Prozessor einschließt, wobei der Prozessor programmiert ist, basierend auf der Änderung des Winkelabtastsignals eine entsprechende Änderung in einer Richtung des Ultraschallbildgebungsstrahls zu bestimmen. 10

15. Bildgebungssonde nach Anspruch 14, wobei der Prozessor programmiert ist, basierend auf einer Rückmeldung von dem Winkelabtastsignal eine Richtung des Ultraschallbildgebungsstrahls zu steuern. 20

16. Verfahren zum Bestimmen einer Richtung eines Bildgebungsstrahls, der von einer Bildgebungssonde emittiert wird, wobei das Verfahren die folgenden Schritte umfasst: 25

Bereitstellen einer Bildgebungssonde nach einem der Ansprüche 6 bis 10; 30

Bereitstellen eines oder mehrerer elektrischer Impulse an den gemeinsamen elektrischen Kanal, wobei der eine oder die mehreren Impulse ausgewählt werden, um den Ultraschallbildgebungsstrahl und den Winkelabtastultraschallstrahl zu erzeugen; 35

Empfangen eines elektrischen Signals auf dem gemeinsamen elektrischen Kanal, wobei das elektrische Signal als Antwort auf den reflektierten Ultraschallstrahl vom Winkelabtastultraschallwandler (100) und als Antwort auf die reflektierte Ultraschallbildgebungsenergie vom Bildgebungsultraschallwandler erzeugt wird; 40

Demultiplexen des elektrischen Signals und Extrahieren des Winkelabtastsignals; und 45

Inbeziehungsetzen des Winkelabtastsignals mit einer Richtung des Ultraschallbildgebungsstrahls.

17. Verfahren nach Anspruch 16, wobei der Schritt des Inbeziehungsetzens des Winkelabtastsignals mit einer Richtung des Ultraschallbildgebungsstrahls durch Vergleichen einer Intensität des Winkelabtastsignals und einer Zeitverzögerung des Winkelabtastsignals mit einem vorbestimmten Wert durchgeführt wird. 50

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Revendications

1. Sonde d'imagerie comprenant :

5 un corps longitudinal (44) ;
un premier transducteur à ultrasons (105) prévu dans ledit corps longitudinal (44), dans laquelle ledit premier transducteur à ultrasons (105) est situé à distance d'une extrémité proximale dudit corps longitudinal (44) et dans laquelle ledit premier transducteur à ultrasons (105) est configuré pour fournir un faisceau d'imagerie ultrasonore dans une région située à l'extérieur dudit corps longitudinal (44) et pour recevoir de l'énergie d'imagerie ultrasonore réfléchie provenant de la région ;
un second transducteur à ultrasons (100) logé dans ledit corps longitudinal (44) ; et
des chemins électriquement conducteurs s'étendant à travers ledit corps longitudinal (44) et définissant un canal électrique commun ;
dans laquelle ledit premier transducteur à ultrasons (105) et ledit second transducteur à ultrasons (100) sont connectés audit canal électrique commun, et dans laquelle ledit canal électrique commun peut être connecté électriquement à un système de traitement d'image (49) ;
dans laquelle ledit premier transducteur à ultrasons (105) et ledit second transducteur à ultrasons (100) présentent chacun des largeurs de bande spectrale ne se chevauchant pas en majeure partie ;
caractérisée en ce que ladite sonde d'imagerie comprend en outre un ensemble d'imagerie (50) logé dans ledit corps longitudinal (44), dans laquelle ledit premier transducteur à ultrasons (105) est prévu dans ledit ensemble d'imagerie (50) ;
dans laquelle ledit ensemble d'imagerie (50) comprend un élément mobile (101) pour balayer une orientation angulaire du faisceau d'imagerie ultrasonore ; et
dans laquelle ledit second transducteur à ultrasons (100) est un transducteur à ultrasons à détection d'angle (100) configuré pour générer un faisceau ultrasonore à détection d'angle et générer un signal de détection d'angle associé à une orientation angulaire dudit élément mobile (101) par rapport à un axe longitudinal dudit corps longitudinal (44).
2. Sonde d'imagerie selon la revendication 1, dans laquelle ledit second transducteur à ultrasons (100) est monté sur ledit premier transducteur à ultrasons (105).
3. Sonde d'imagerie selon la revendication 1 ou 2, dans laquelle ledit premier transducteur à ultrasons (105)

est configuré pour pivoter autour d'un axe de pivotement.

4. Sonde d'imagerie selon l'une quelconque des revendications 1 à 3, dans laquelle le faisceau d'imagerie à ultrasons est un premier faisceau ultrasonore, ledit second transducteur à ultrasons (100) est un transducteur d'imagerie configuré pour produire un faisceau d'imagerie ultrasonore supplémentaire.

5. Sonde d'imagerie selon la revendication 4, dans laquelle ledit second transducteur à ultrasons (100) est configuré pour fournir le faisceau d'imagerie ultrasonore supplémentaire dans une direction sensiblement anti-colinéaire à celle du premier faisceau ultrasonore.

6. Sonde d'imagerie selon la revendication 1, dans laquelle ledit ensemble d'imagerie (50) comprend en outre un substrat à réflexion acoustique, dans laquelle ledit transducteur à ultrasons à détection d'angle (100) est configuré pour diriger un faisceau ultrasonore à détection d'angle vers ledit substrat à réflexion acoustique et pour recevoir un faisceau ultrasonore réfléchi par ledit substrat à réflexion acoustique, de sorte qu'un signal de détection d'angle produit par ledit transducteur à ultrasons à détection d'angle (100) en réponse au faisceau ultrasonore réfléchi soit détectable sur ledit canal électrique commun, et dans laquelle ledit substrat à réflexion acoustique est positionné par rapport audit élément mobile (101) de sorte qu'une modification de l'orientation dudit élément mobile (101) par rapport à un axe longitudinal dudit corps longitudinal (44) produit une modification du signal de détection d'angle.

7. Sonde d'imagerie selon la revendication 6, dans laquelle ledit substrat à réflexion acoustique est configuré de telle sorte que la modification du signal de détection d'angle inclut un retard relatif du signal de détection d'angle.

8. Sonde d'imagerie selon la revendication 6, dans laquelle ledit premier transducteur à ultrasons (105) et ledit transducteur à ultrasons à détection d'angle (100) forment au moins une partie dudit élément mobile (101) ;
dans laquelle ledit substrat à réflexion acoustique comprend un profil de surface incurvé, une courbure dudit profil de surface incurvée étant sélectionnée de telle sorte qu'une déviation dudit élément mobile (101) produit une modification du retard relatif du signal de détection d'angle ;
et ledit profil de surface incurvée étant sélectionné de sorte qu'une distance entre ledit transducteur à ultrasons à détection d'angle (100) et ledit substrat à réflexion acoustique, telle que déterminée le long d'un trajet de faisceau du faisceau ultrasonore à détection d'angle, varie sur une plage angulaire définie dudit élément pivotant.

9. Sonde d'imagerie selon la revendication 6, dans laquelle ledit élément mobile (101) comprend un premier élément pouvant être dévié (101) couplé mécaniquement à un second élément pouvant être dévié (114), de sorte qu'un changement d'orientation du premier élément pouvant être dévié (101) produit une changement correspondant d'une orientation dudit second élément pouvant être dévié (114), et dans laquelle un changement d'orientation dudit second élément pouvant être dévié (114) produit un changement de direction du faisceau d'imagerie ultrasonore.

10. Sonde d'imagerie selon la revendication 6, dans laquelle ledit transducteur à ultrasons à détection d'angle (100) est positionné de telle sorte que le faisceau ultrasonore à détection d'angle est contraint d'être dirigé approximativement perpendiculairement à une surface dudit substrat à réflexion acoustique.

11. Sonde d'imagerie selon l'une quelconque des revendications 6 à 10, comprenant en outre un sous-système de fourniture et de détection pour fournir de l'énergie électrique audit premier transducteur à ultrasons (105) et audit transducteur à ultrasons à détection d'angle (100), et pour détecter les signaux électriques détectés par ledit premier transducteur à ultrasons (105) et ledit transducteur à ultrasons à détection d'angle (100).

12. Sonde d'imagerie selon la revendication 11, dans laquelle ledit premier transducteur à ultrasons (105) et ledit transducteur à ultrasons à détection d'angle (100) sont chacun **caractérisés par** des largeurs de bande spectrale ne se chevauchant pas, et dans laquelle ledit sous-système de fourniture et de détection est configuré pour fournir de l'énergie électrique à large bande audit premier transducteur à ultrasons (105) et audit transducteur à ultrasons à détection d'angle (100) de telle sorte qu'un spectre de l'énergie électrique à large bande chevauche une largeur de bande spectrale dudit premier transducteur à ultrasons (105) et dudit transducteur à ultrasons à détection d'angle (100).

13. Sonde d'imagerie selon la revendication 11, dans laquelle ledit premier transducteur à ultrasons (105) et ledit transducteur à ultrasons à détection d'angle (100) sont chacun **caractérisés par** des largeurs de bande spectrale ne se chevauchant pas, et dans laquelle ledit sous-système de fourniture et de détection est configuré pour fournir de l'énergie électrique audit premier transducteur à ultrasons (105) et audit transducteur à ultrasons à détection d'angle (100)

de sorte qu'un spectre de l'énergie électrique comprend une première composante spectrale dans une largeur de bande spectrale dudit premier transducteur à ultrasons (105) et une seconde composante spectrale dans une largeur de bande spectrale dudit transducteur à ultrasons à détection d'angle (100). 5

14. Sonde d'imagerie selon la revendication 12 ou 13, dans laquelle ledit sous-système de fourniture et de détection comprend en outre un processeur, ledit processeur étant programmé pour déterminer, en fonction du changement du signal de détection d'angle, un changement correspondant dans une direction du faisceau d'imagerie ultrasonore. 10

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15. Sonde d'imagerie selon la revendication 14, dans laquelle ledit processeur est programmé pour commander une direction du faisceau d'imagerie ultrasonore sur la base des informations provenant du signal de détection d'angle. 20

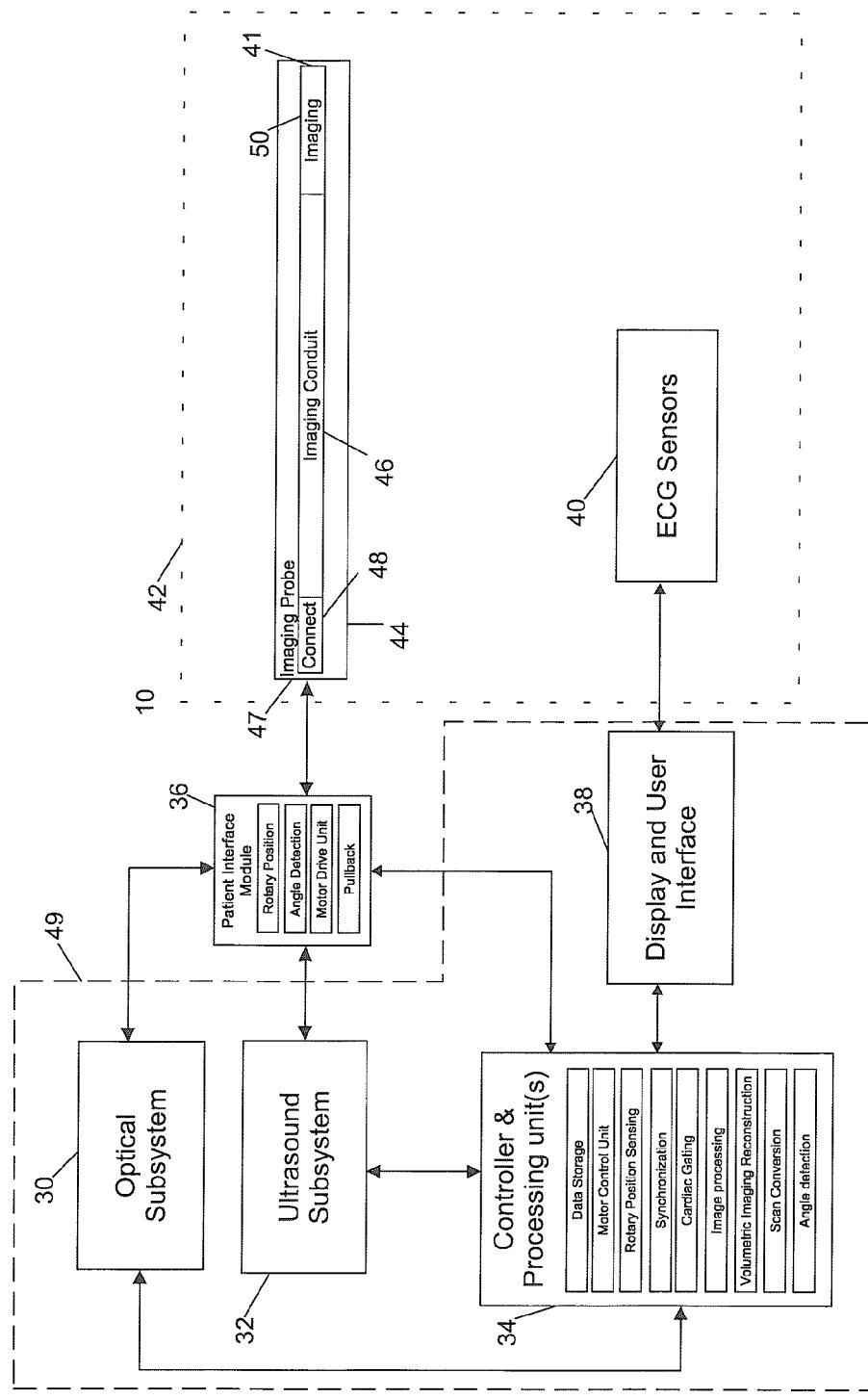
16. Procédé de détermination de la direction d'un faisceau d'imagerie émis par une sonde d'imagerie, le procédé comprenant les étapes consistant à : 25

fournir une sonde d'imagerie selon l'une quelconque des revendications 6 à 10 ;
 fournir une ou plusieurs impulsions électriques au canal électrique commun, la ou les impulsions étant sélectionnées pour générer le faisceau d'imagerie ultrasonore et le faisceau ultrasonore à détection d'angle ;
 recevoir un signal électrique sur le canal électrique commun, le signal électrique étant généré par le transducteur à ultrasons à détection d'angle (100) en réponse au faisceau ultrasonore réfléchi et par le transducteur à ultrasons d'imagerie en réponse à l'énergie d'imagerie ultrasonore réfléchie ;
 démultiplexer le signal électrique et extraire le signal de détection d'angle ; et
 relier le signal de détection d'angle à une direction du faisceau d'imagerie ultrasonore. 30 35 40

17. Procédé selon la revendication 16, dans lequel l'étape consistant à relier le signal de détection d'angle à une direction du faisceau d'imagerie ultrasonore est effectuée en comparant l'une d'une intensité du signal de détection d'angle et d'un retard du signal de détection d'angle à une valeur prédéfinie. 45 50

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FIG. 1



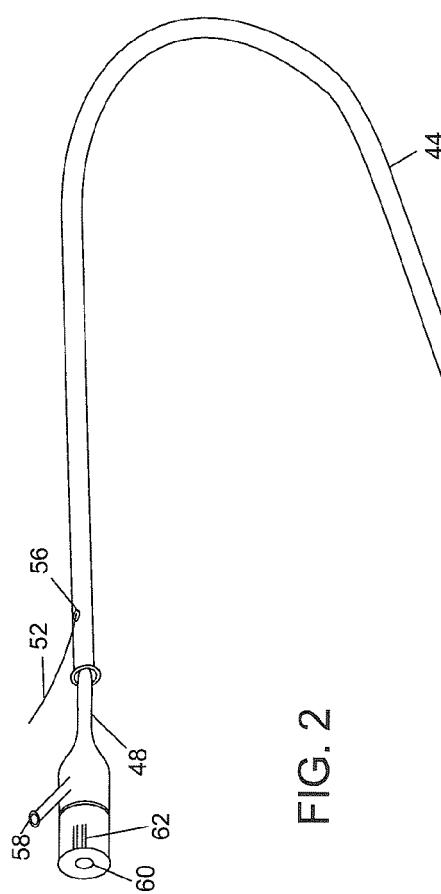


FIG. 2

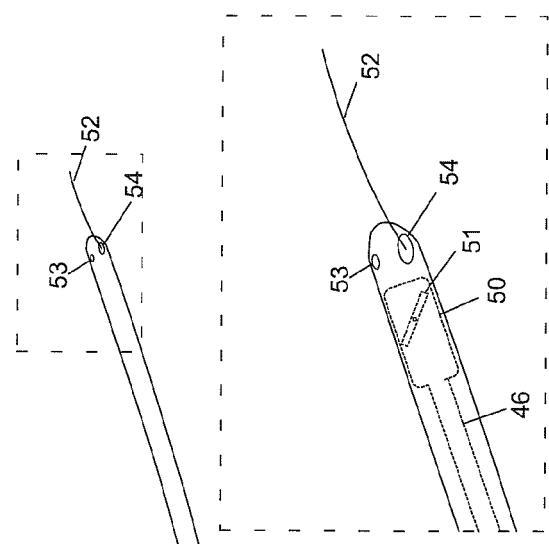


FIG. 2b

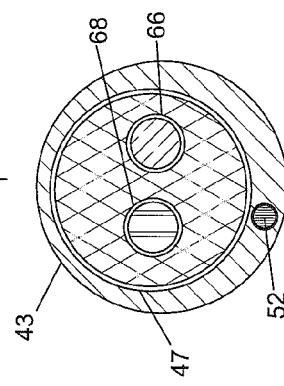


FIG. 2a

FIG. 3a

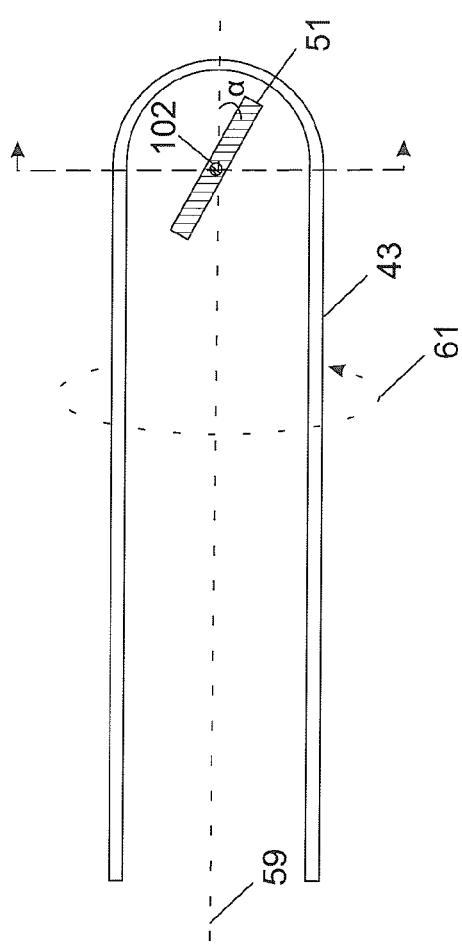


FIG. 3b

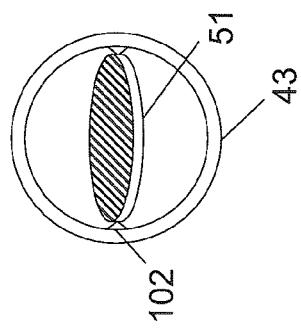


FIG. 3c

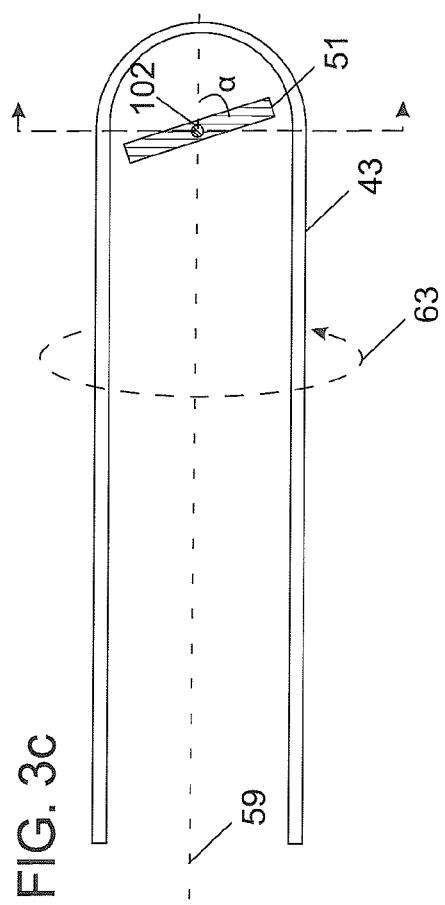


FIG. 3d

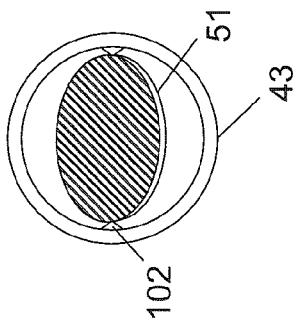


FIG. 3f

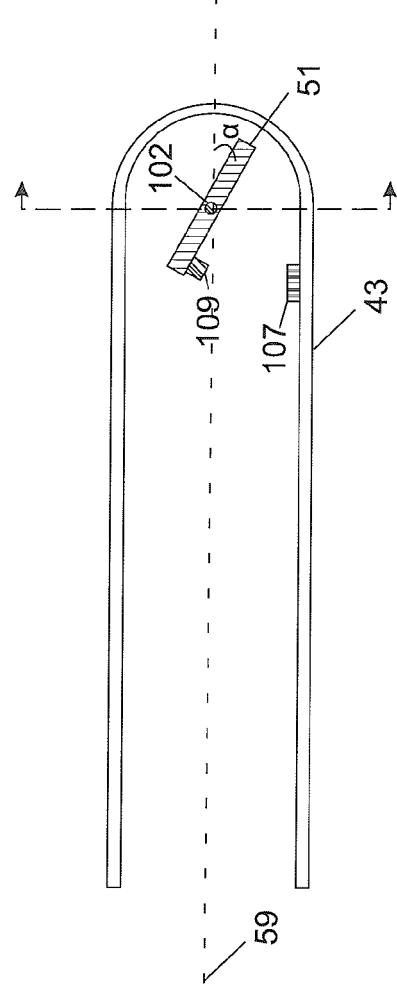
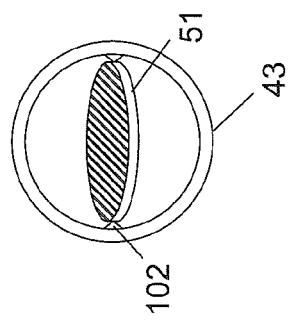
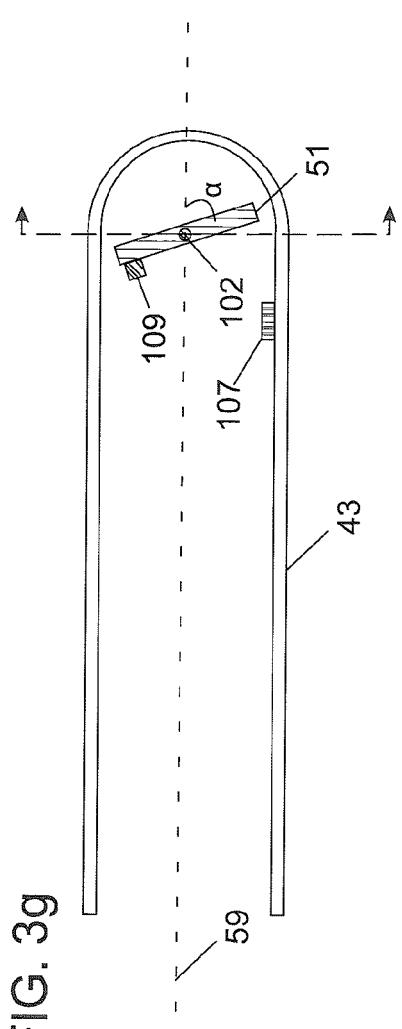
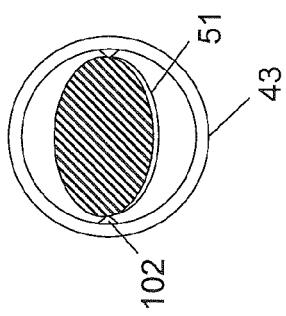


FIG. 3h



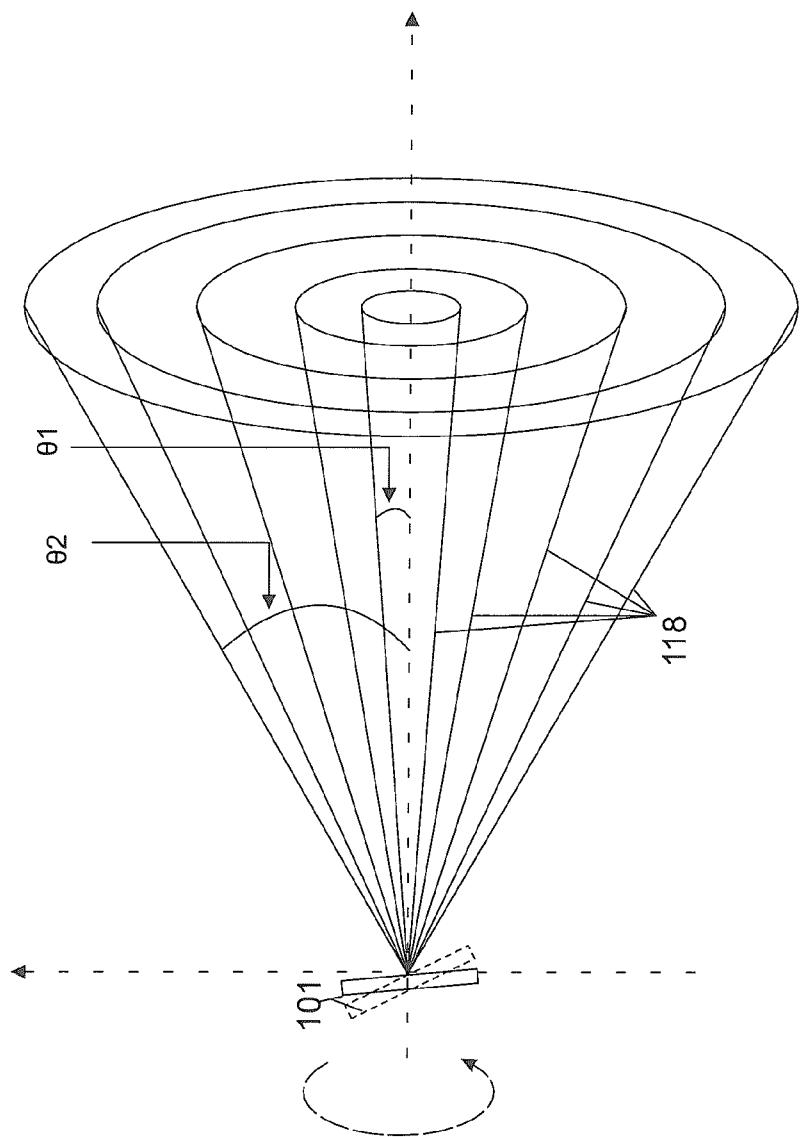


FIG. 3i

FIG. 3j

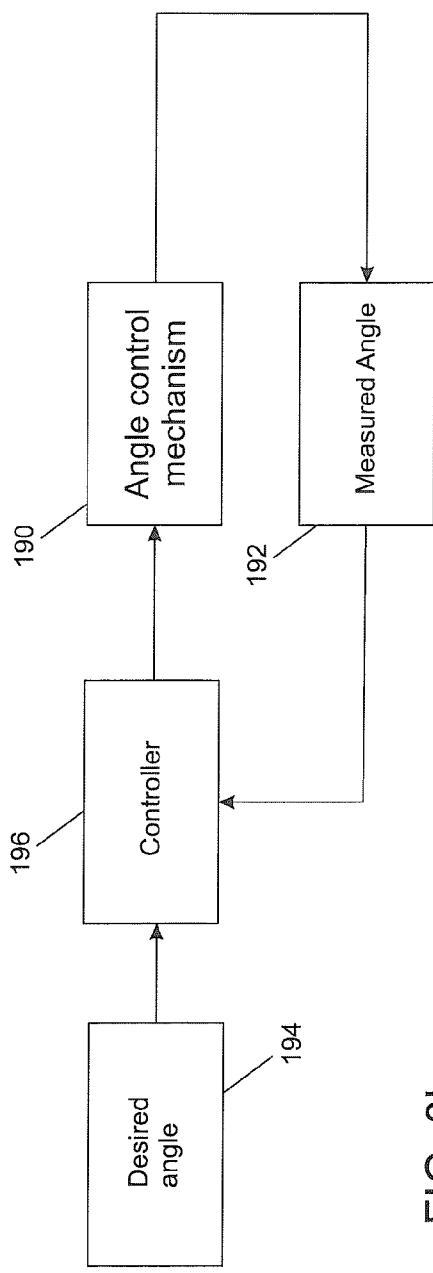


FIG. 3k

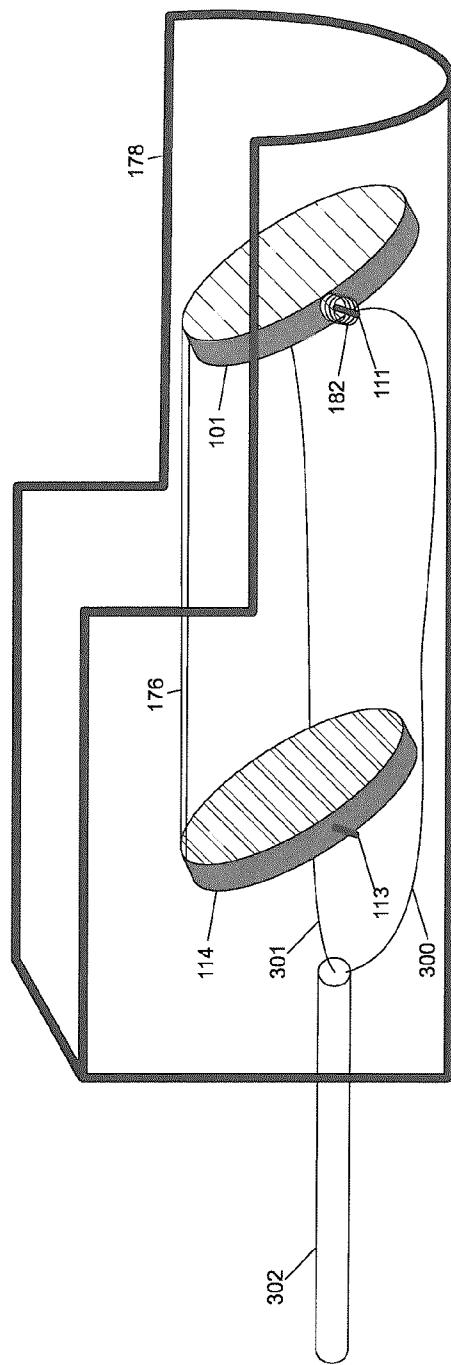


FIG. 4a

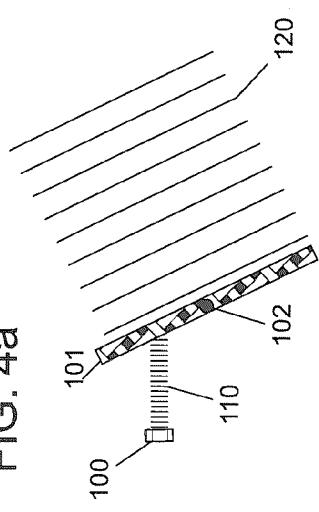


FIG. 4b

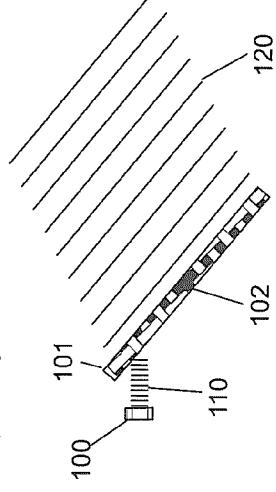


FIG. 4c

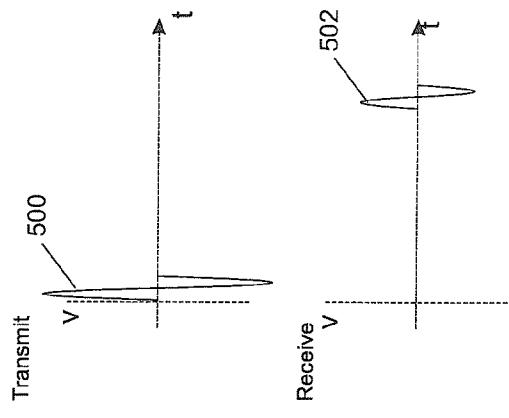


FIG. 4d

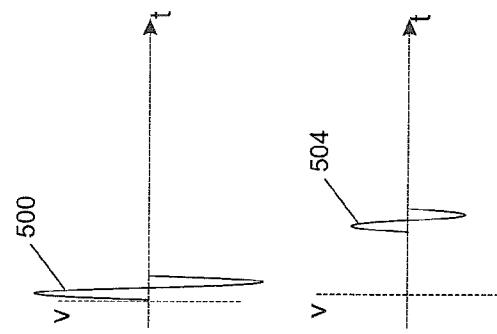


FIG. 4e

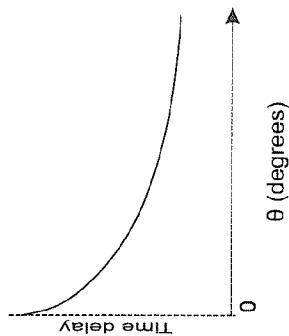


FIG. 4f
FIG. 4g

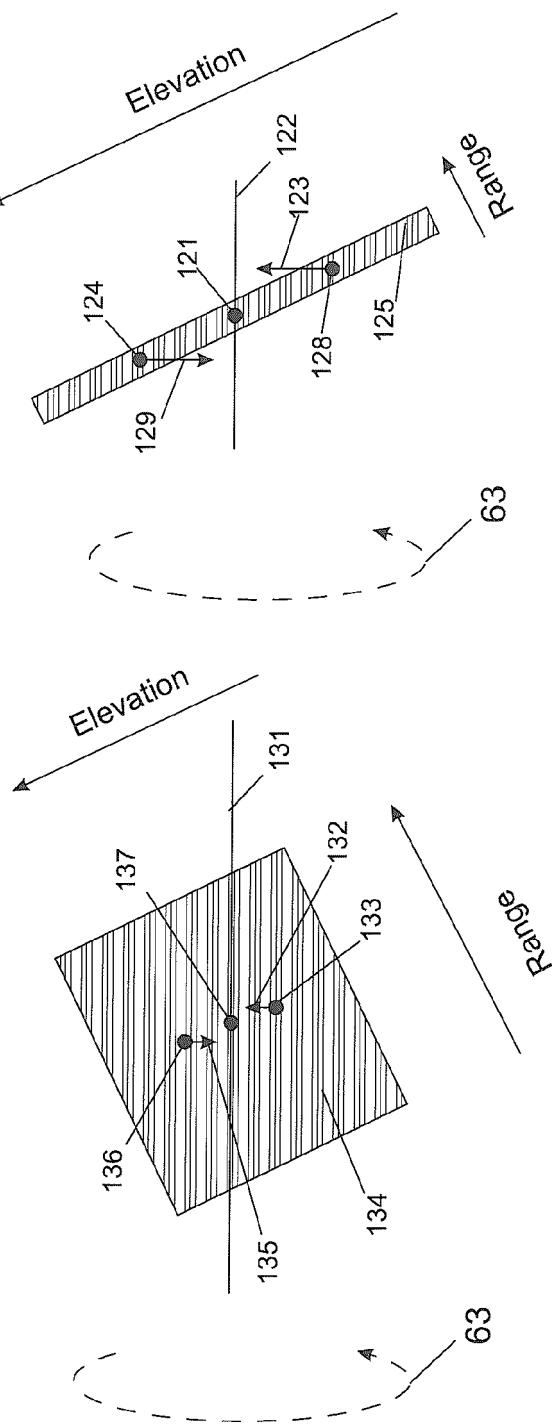


FIG. 5a

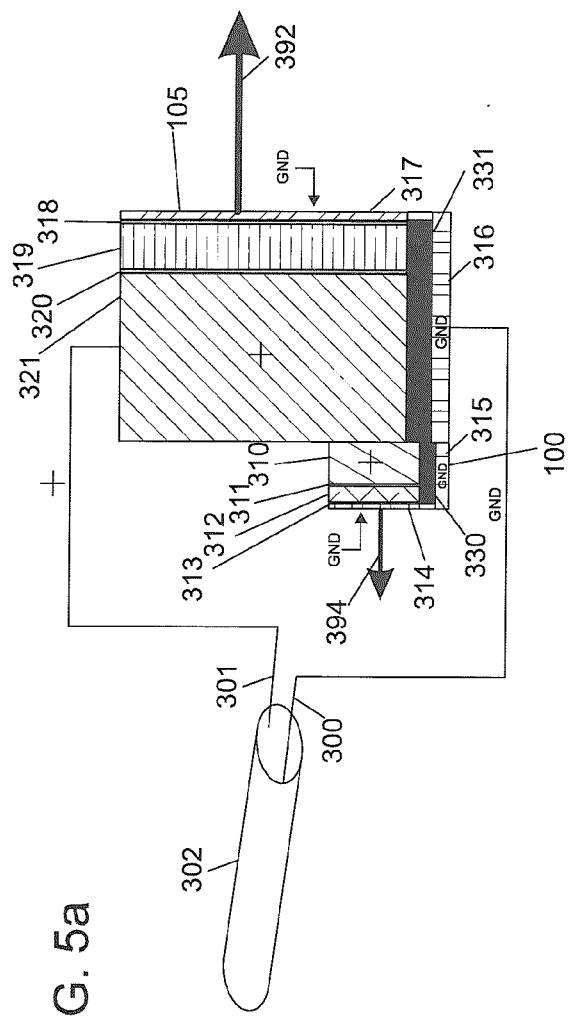


FIG. 5b

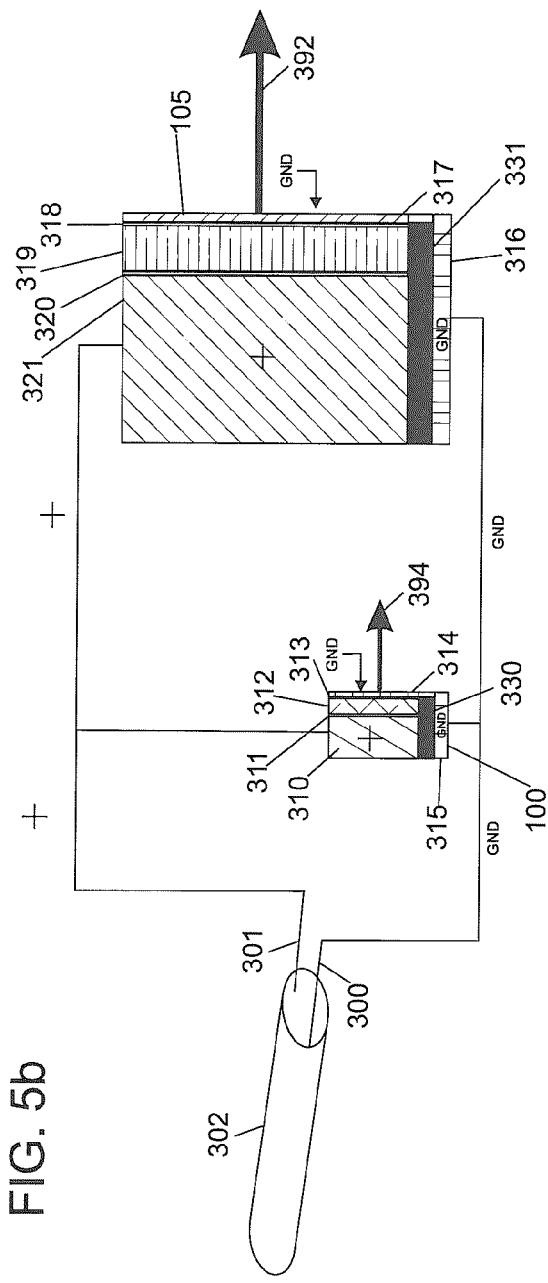


FIG. 5c

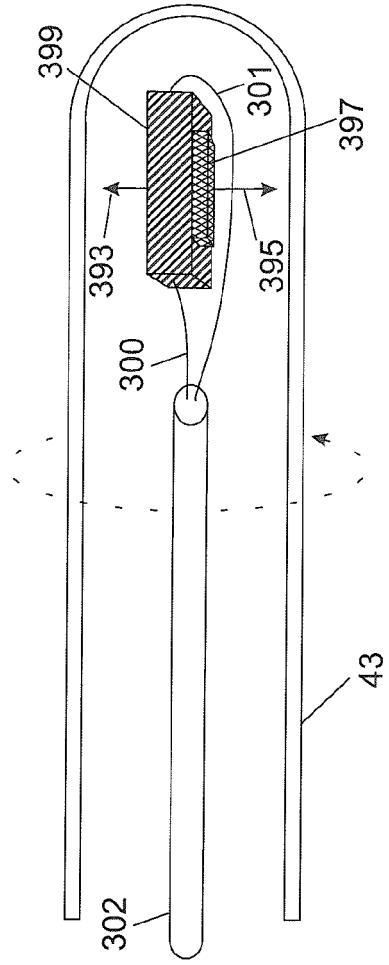


FIG. 5d

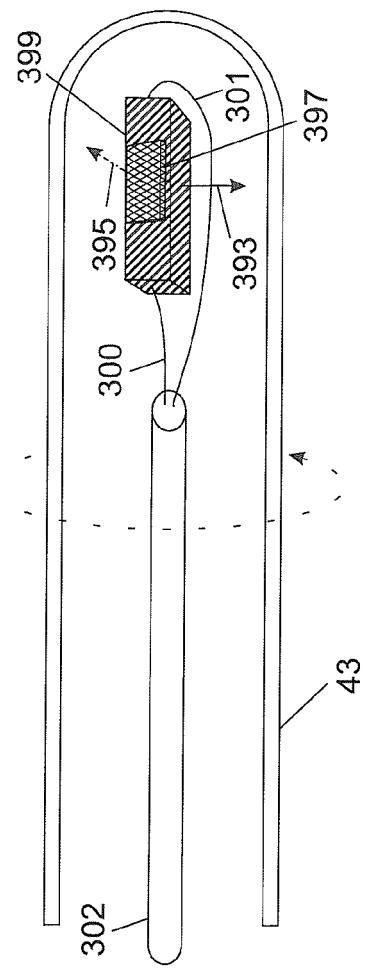


FIG. 5e

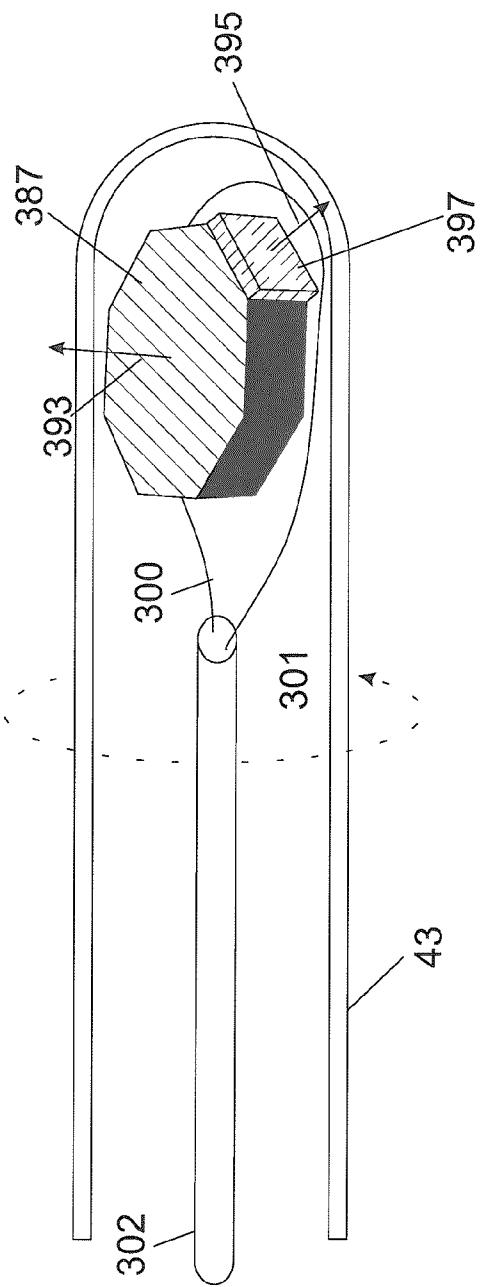


FIG. 5f

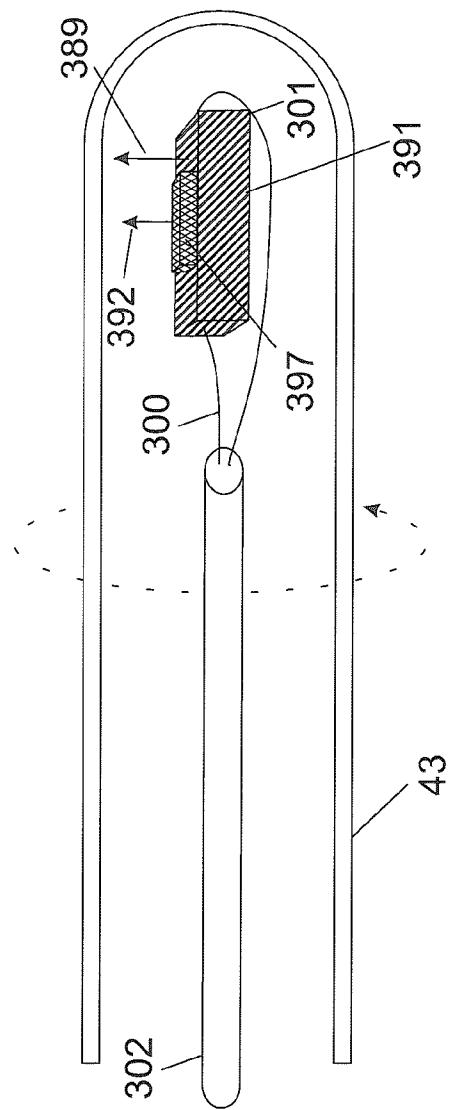


FIG. 5g

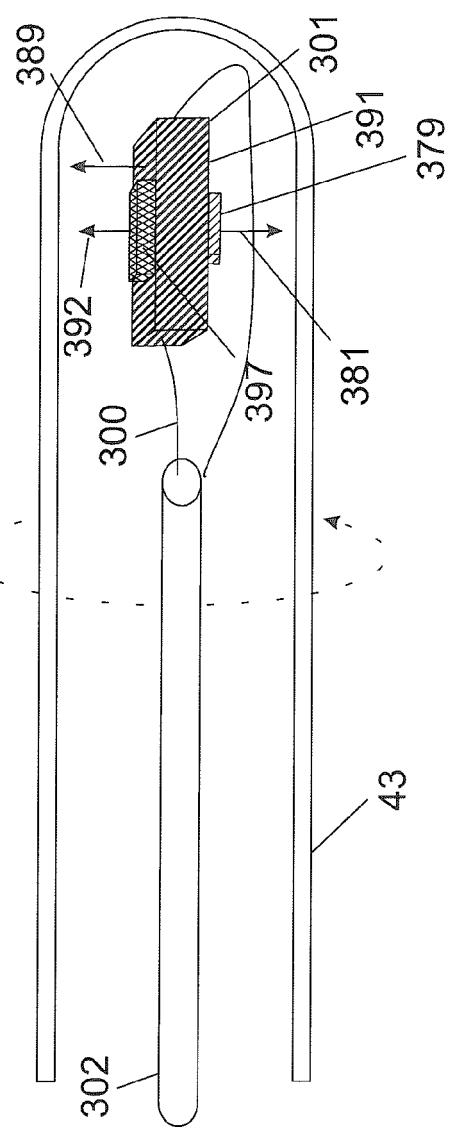


FIG. 5h

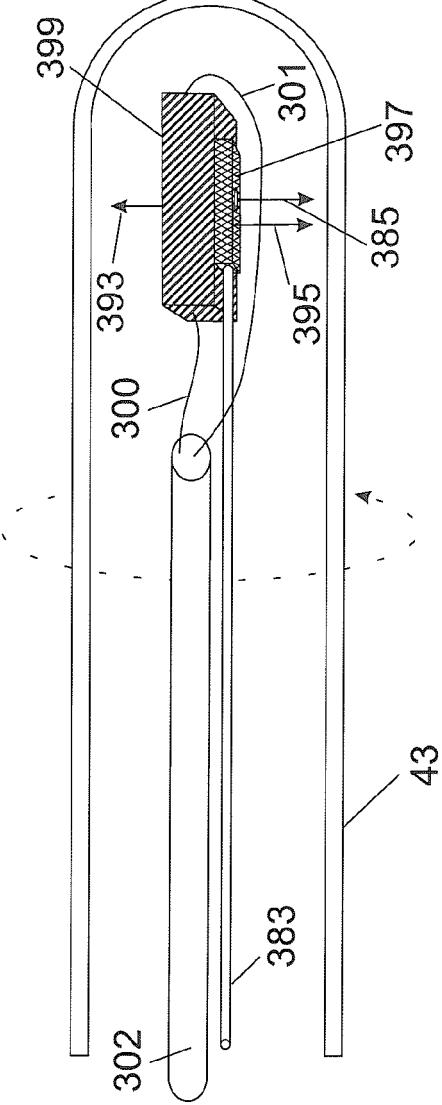
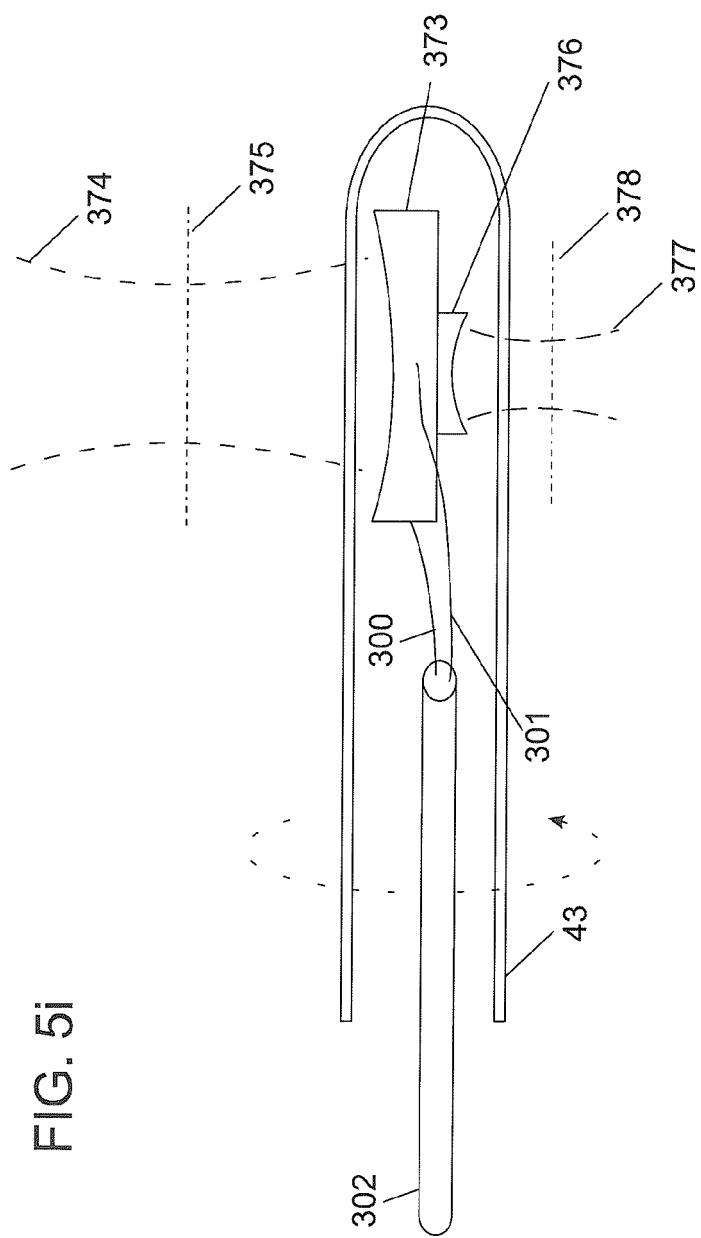


FIG. 5j



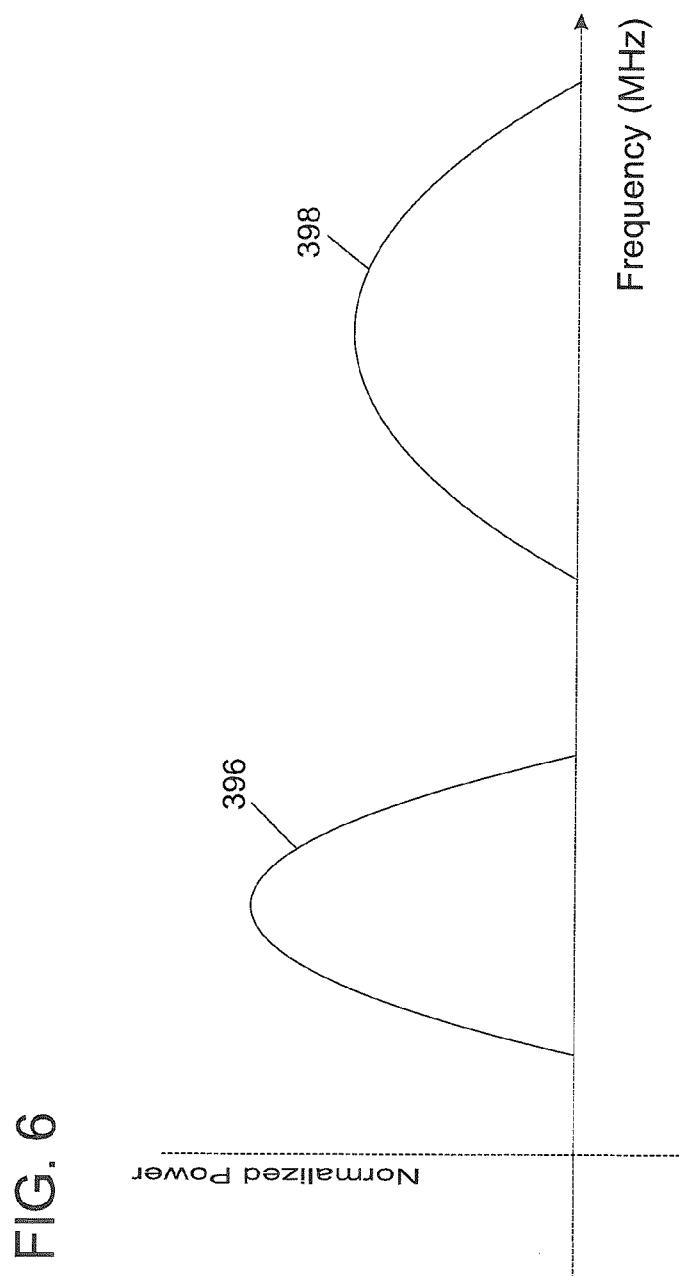
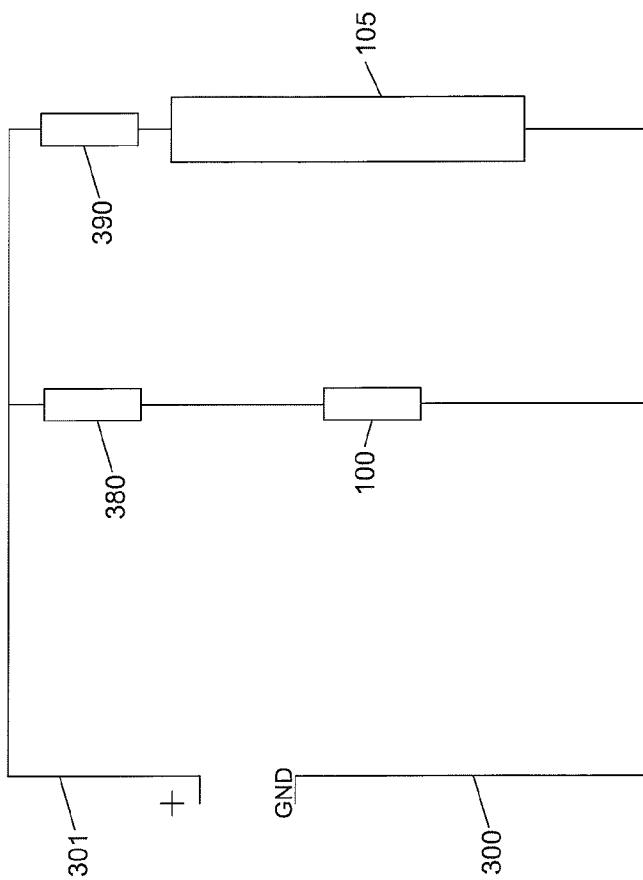


FIG. 7



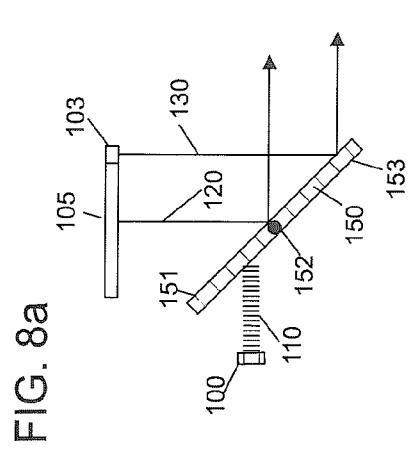


FIG. 8b

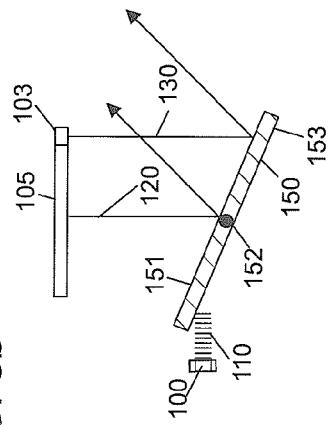


FIG. 8e

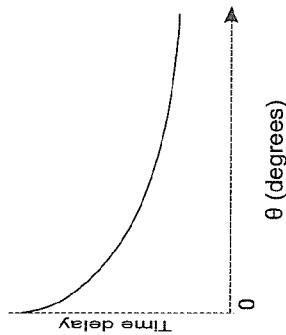


FIG. 8d

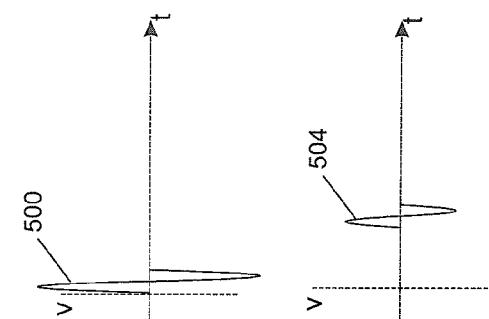


FIG. 8c

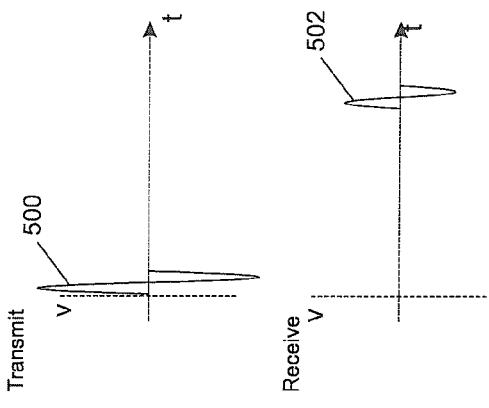
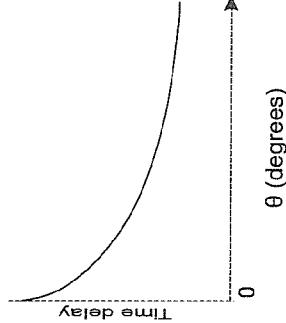


FIG. 8e



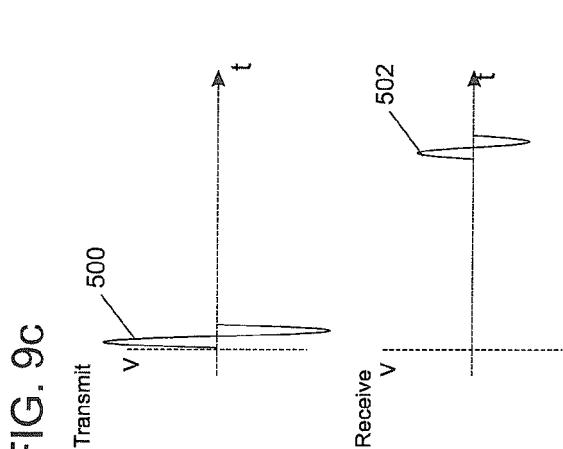
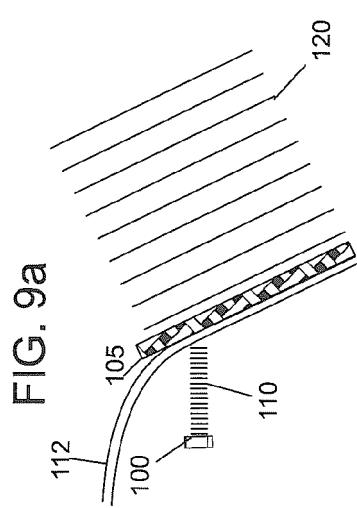


FIG. 9b

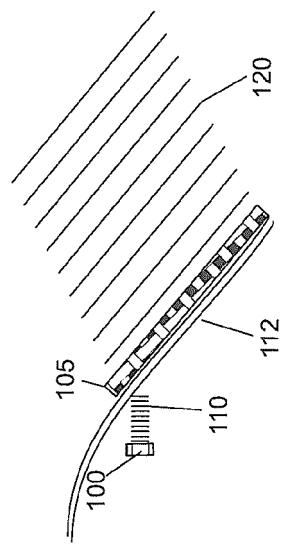


FIG. 9d

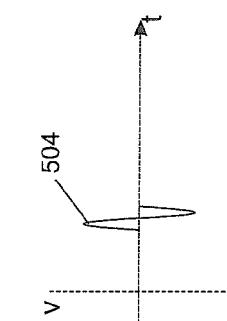
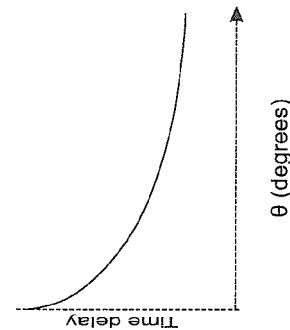
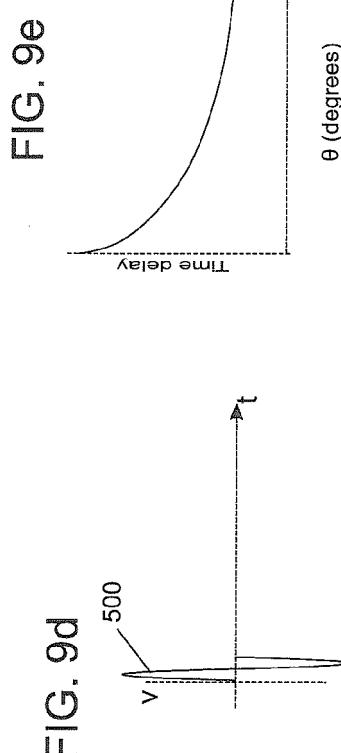


FIG. 10a

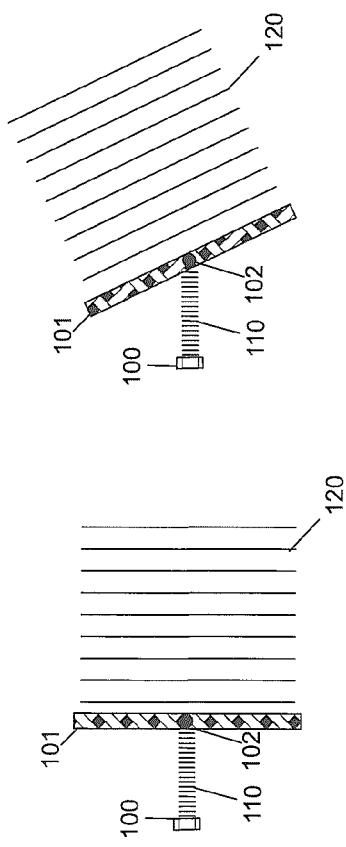


FIG. 10b

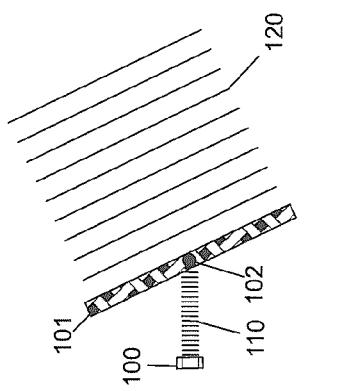


FIG. 10c

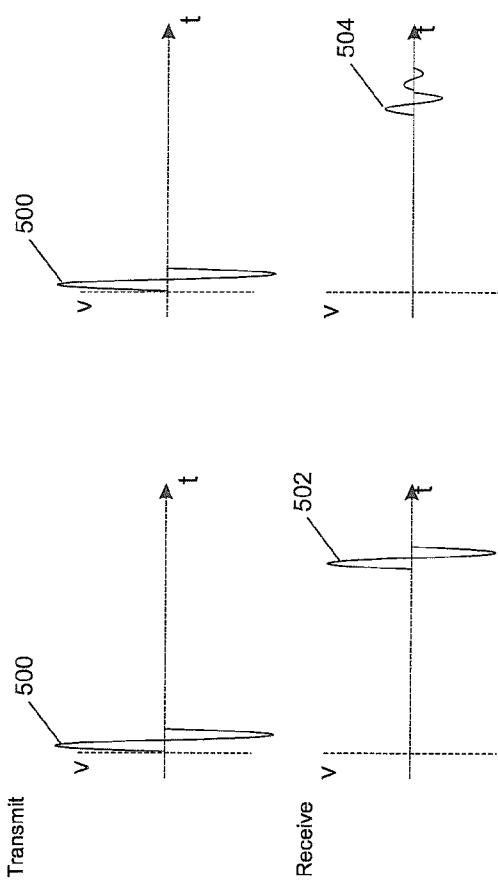


FIG. 10d

θ (degrees)

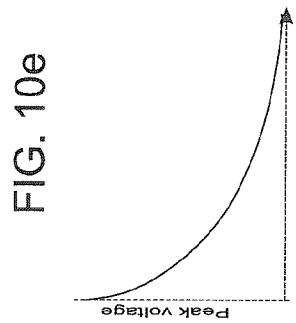


FIG. 10e

FIG. 11a

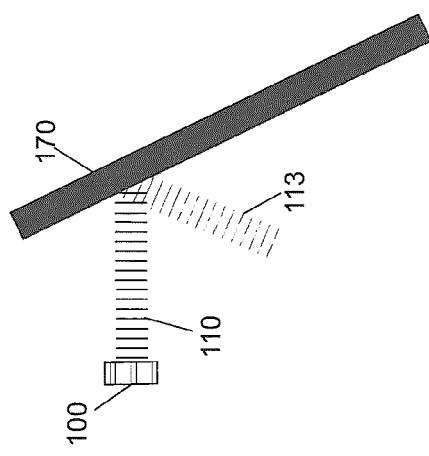


FIG. 11b

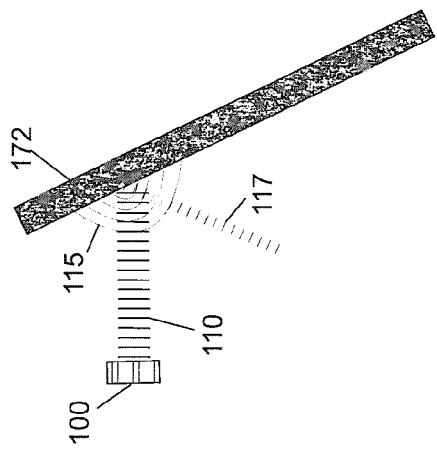


FIG. 11c

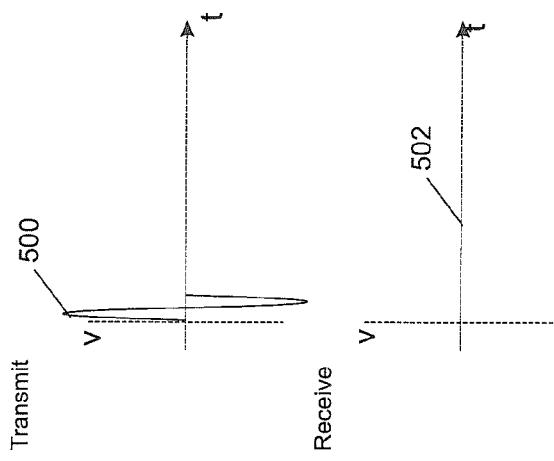


FIG. 11d

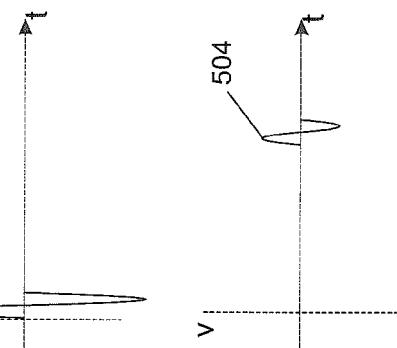


FIG. 12a

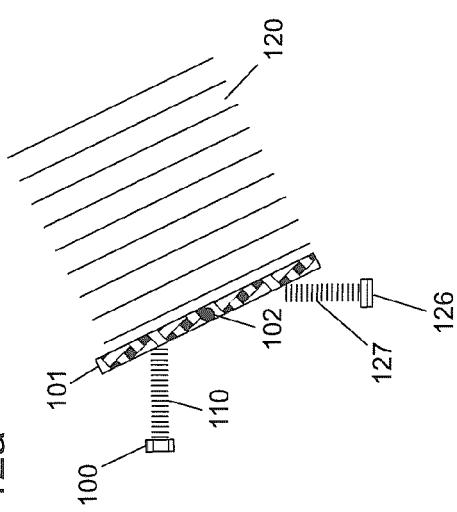


FIG. 12b

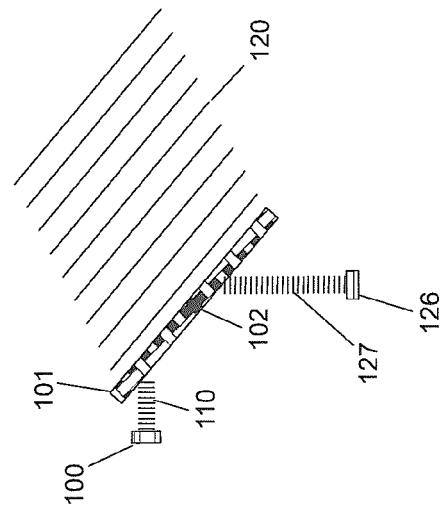


FIG. 12c
Transmit

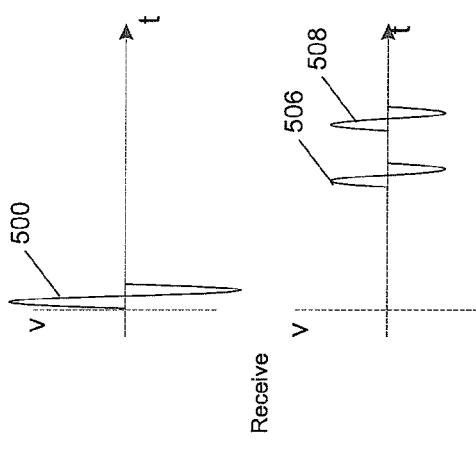


FIG. 12d

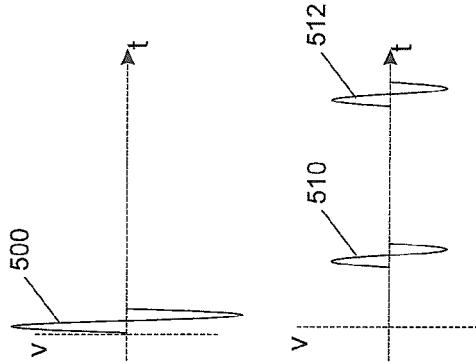


FIG. 13a

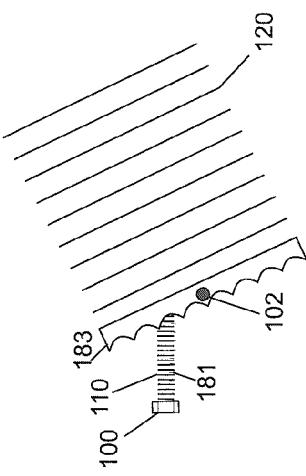


FIG. 13b

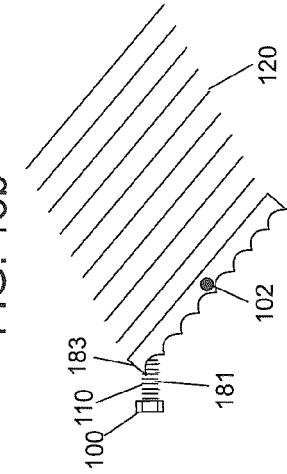


FIG. 13c

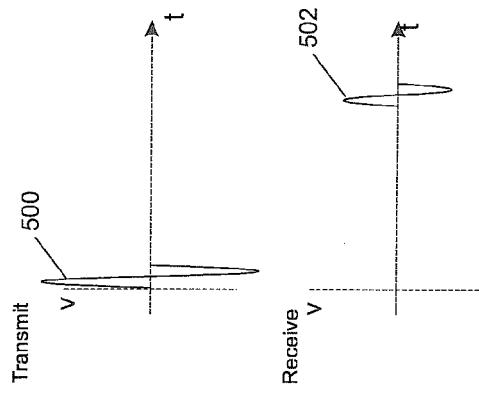


FIG. 13d

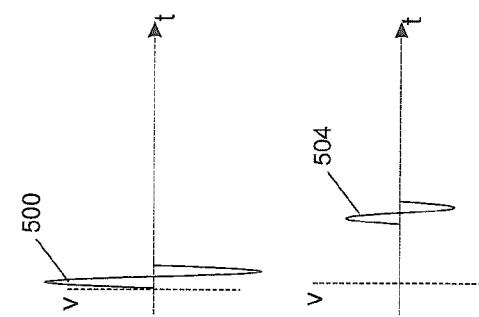
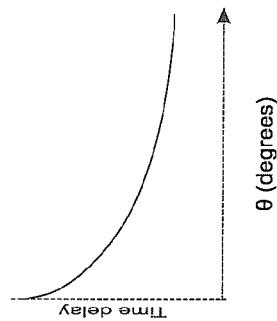


FIG. 13e



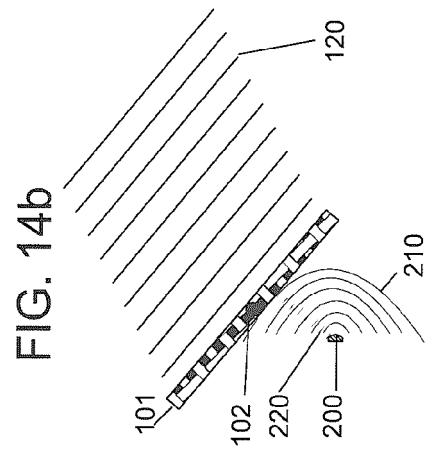
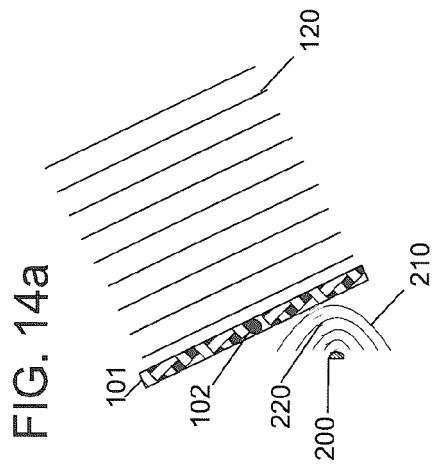


FIG. 14c

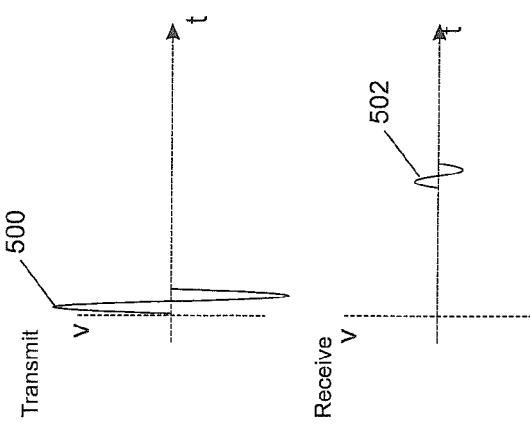


FIG. 14d

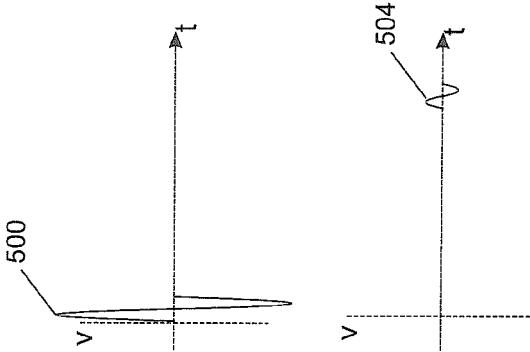


FIG. 15a

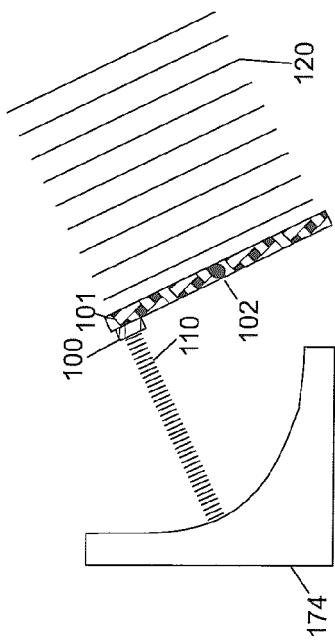


FIG. 15b

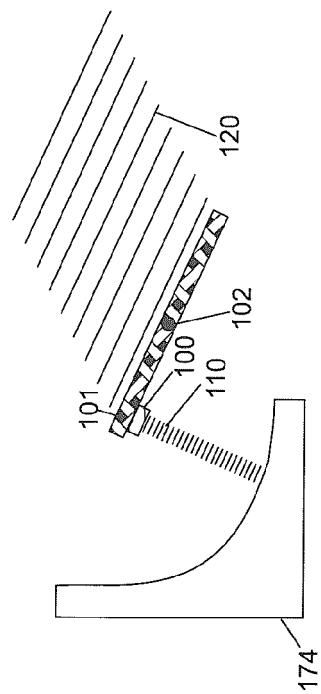


FIG. 15c

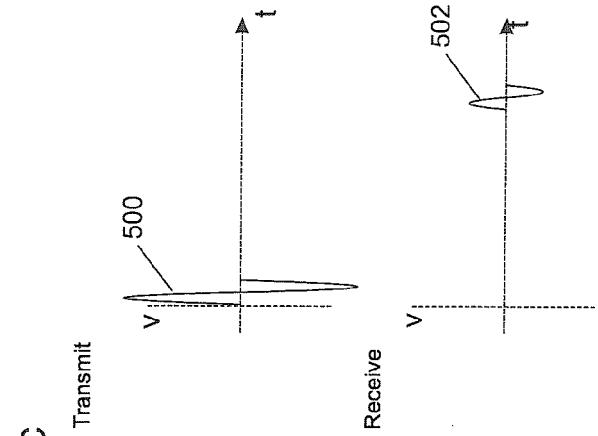


FIG. 15d

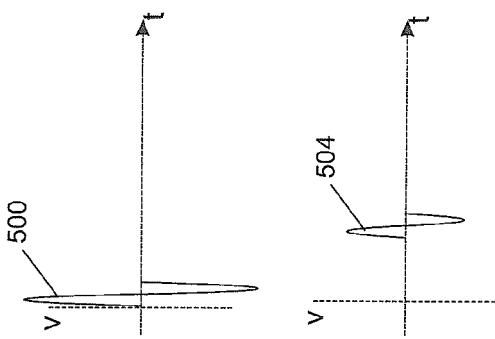


FIG. 15e

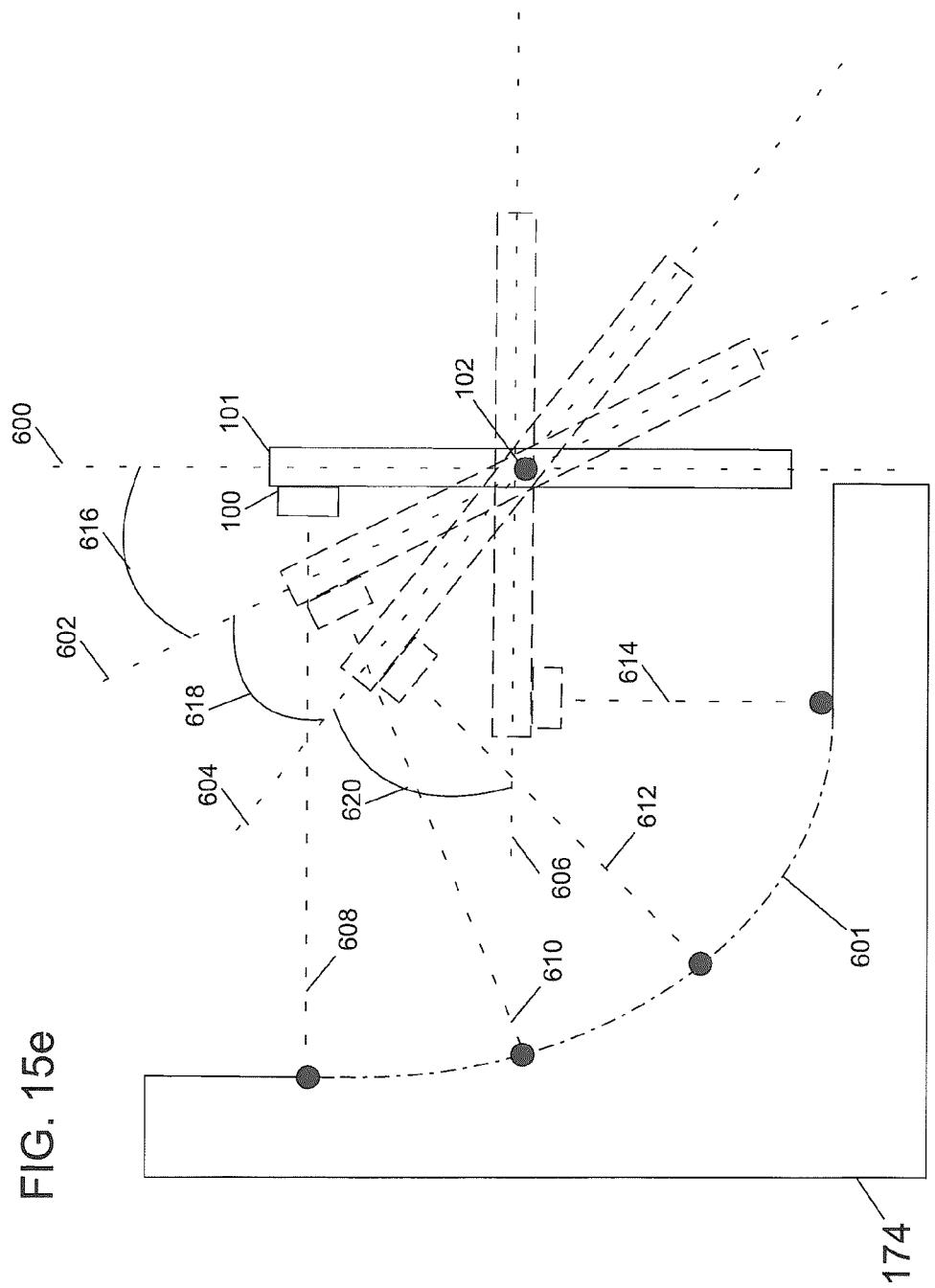


FIG. 16a

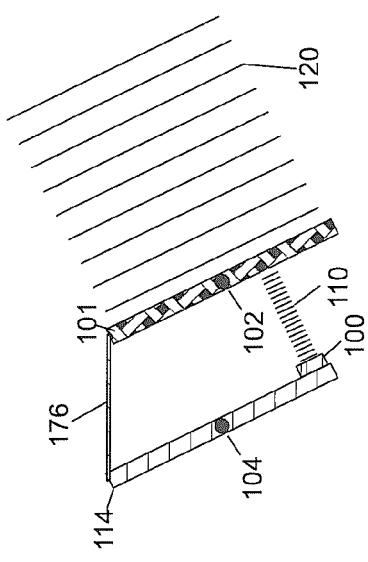


FIG. 16b

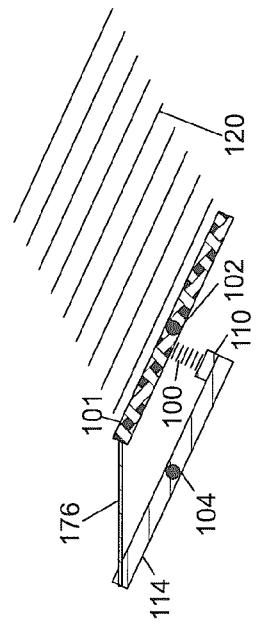


FIG. 16c

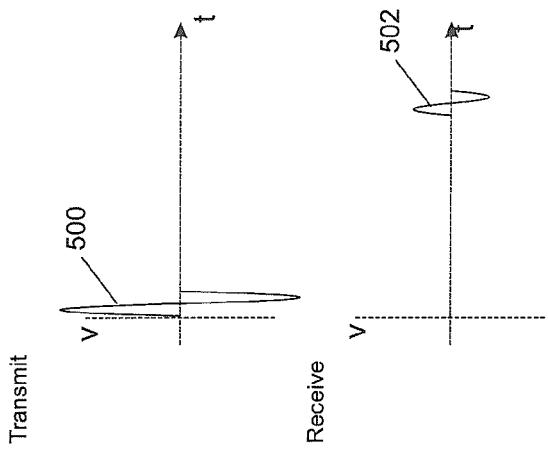
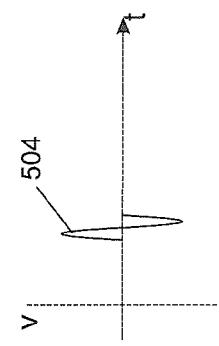
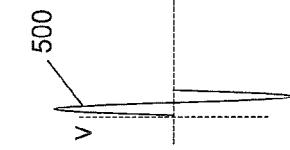
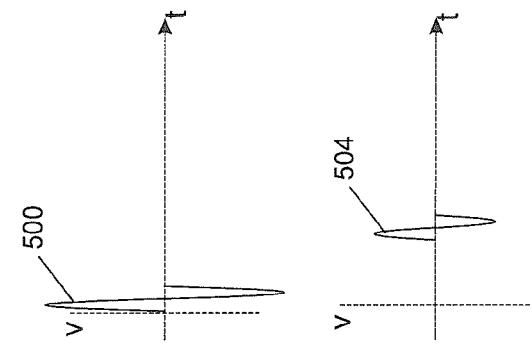


FIG. 16d



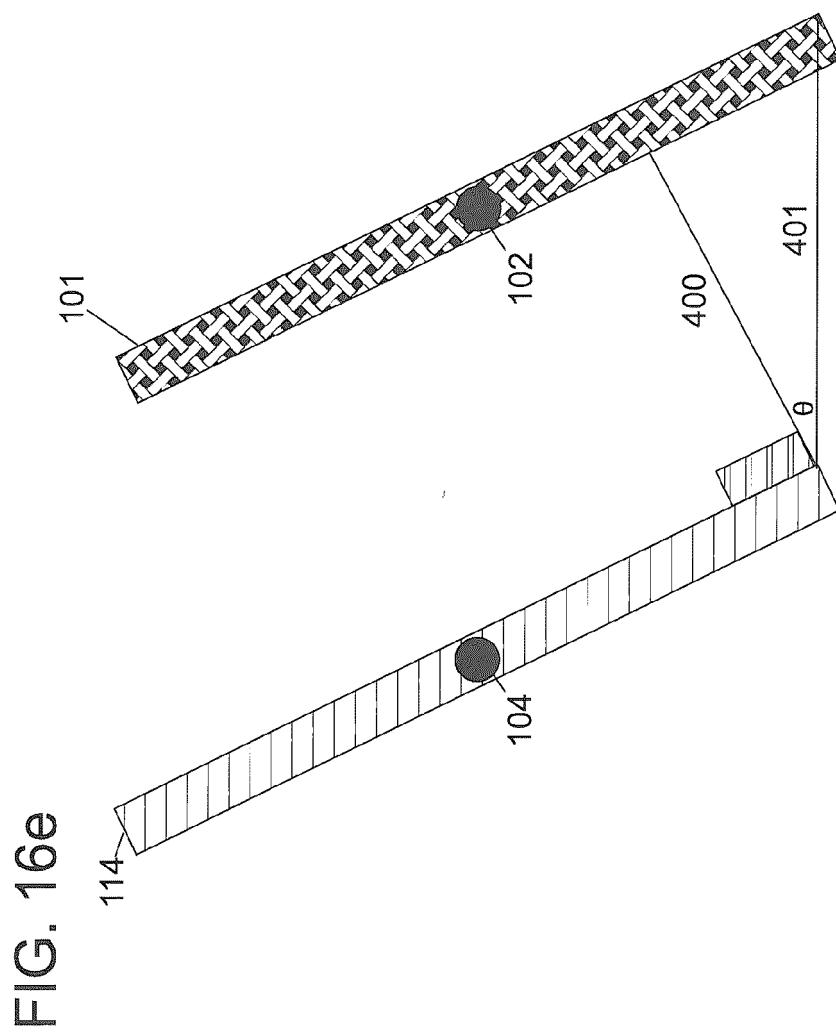


FIG. 16e

FIG. 17a

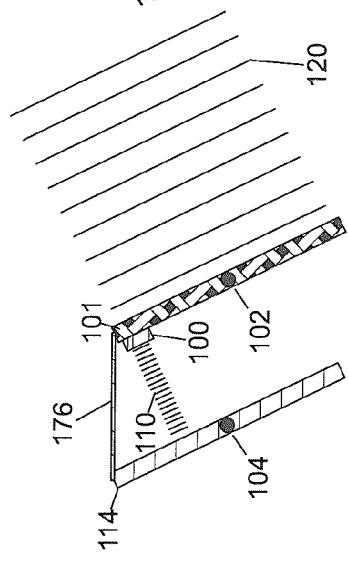


FIG. 17b

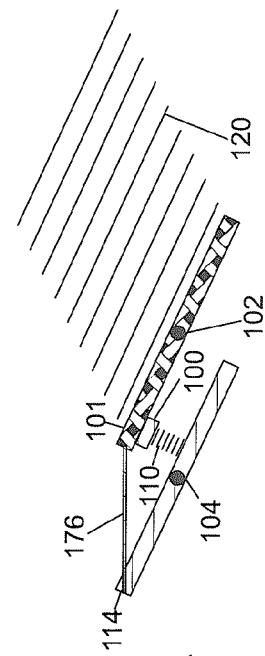


FIG. 17c

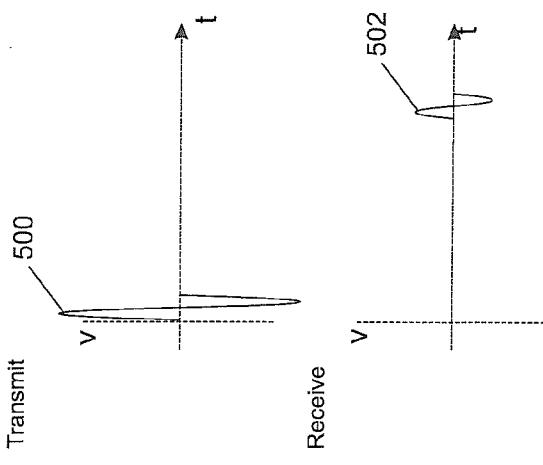


FIG. 17d

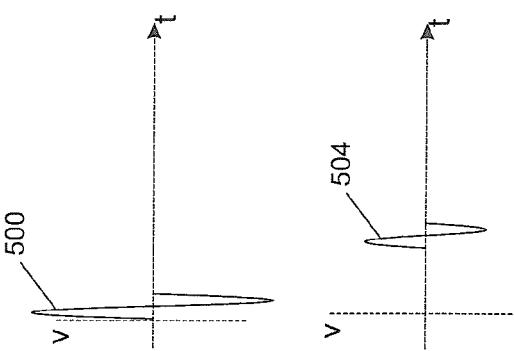


FIG. 18a

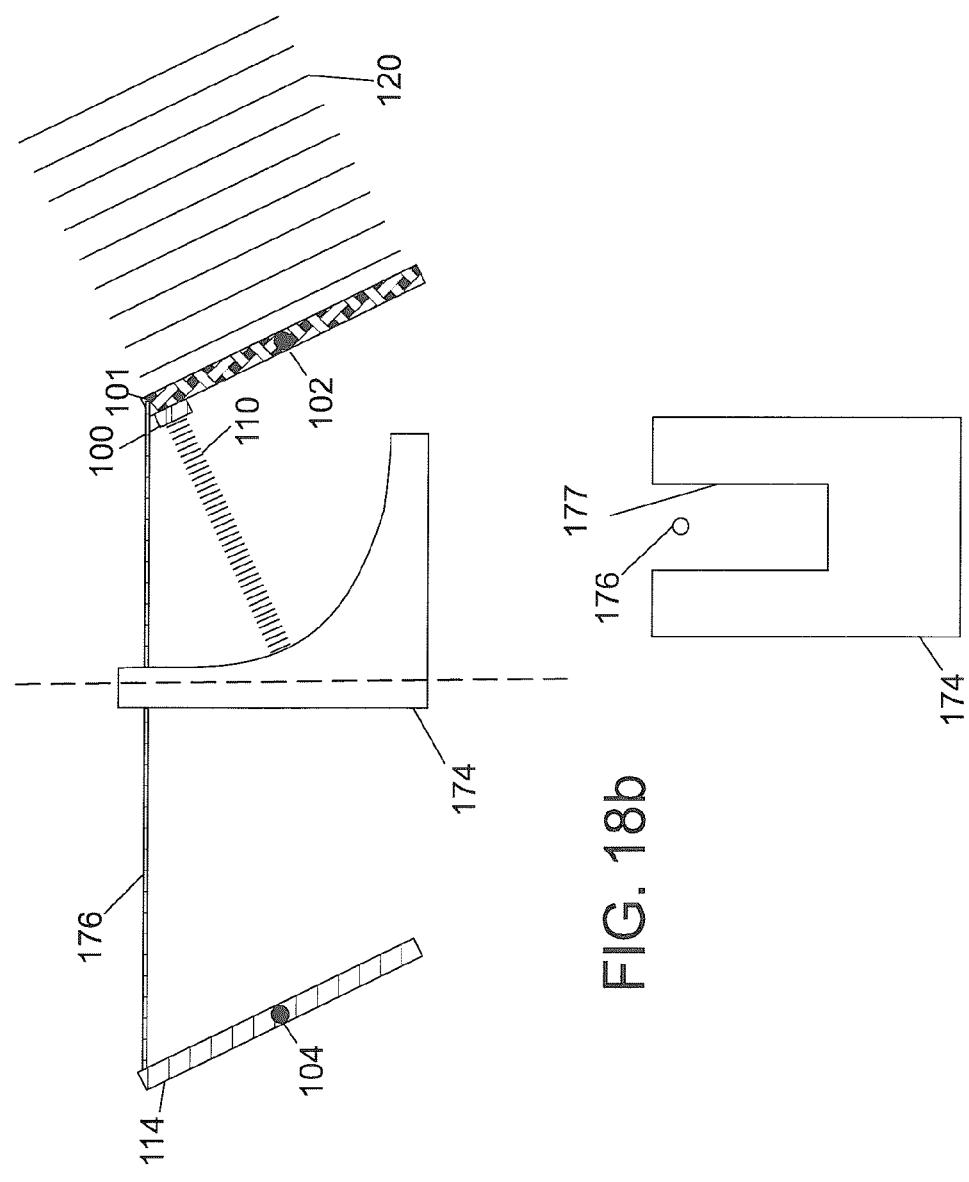


FIG. 18b

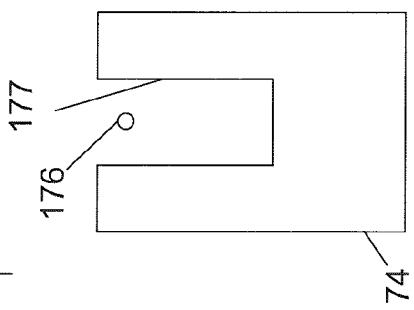


FIG. 18c

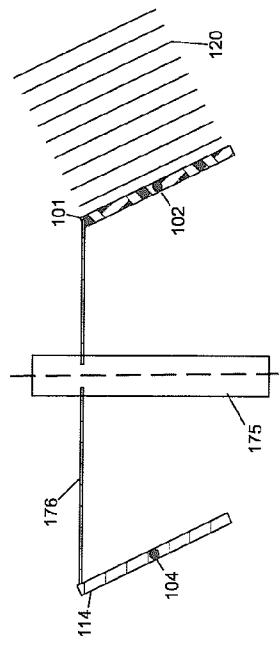


FIG. 18d

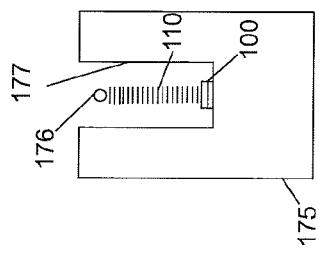


FIG. 18e

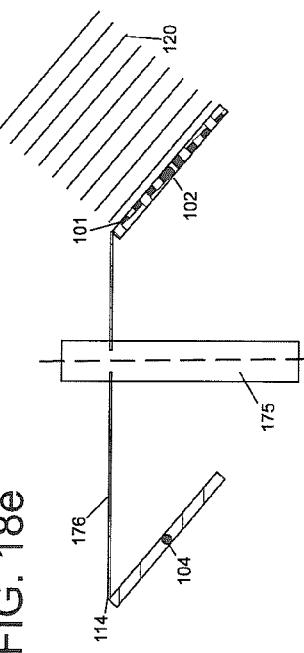


FIG. 18f

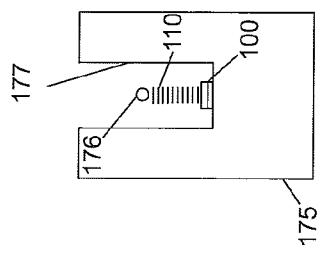


FIG. 18g

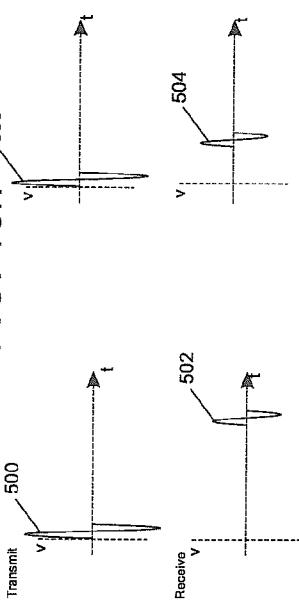


FIG. 18i

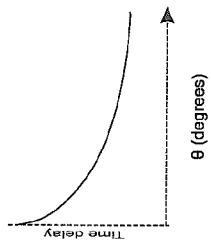


FIG. 19a

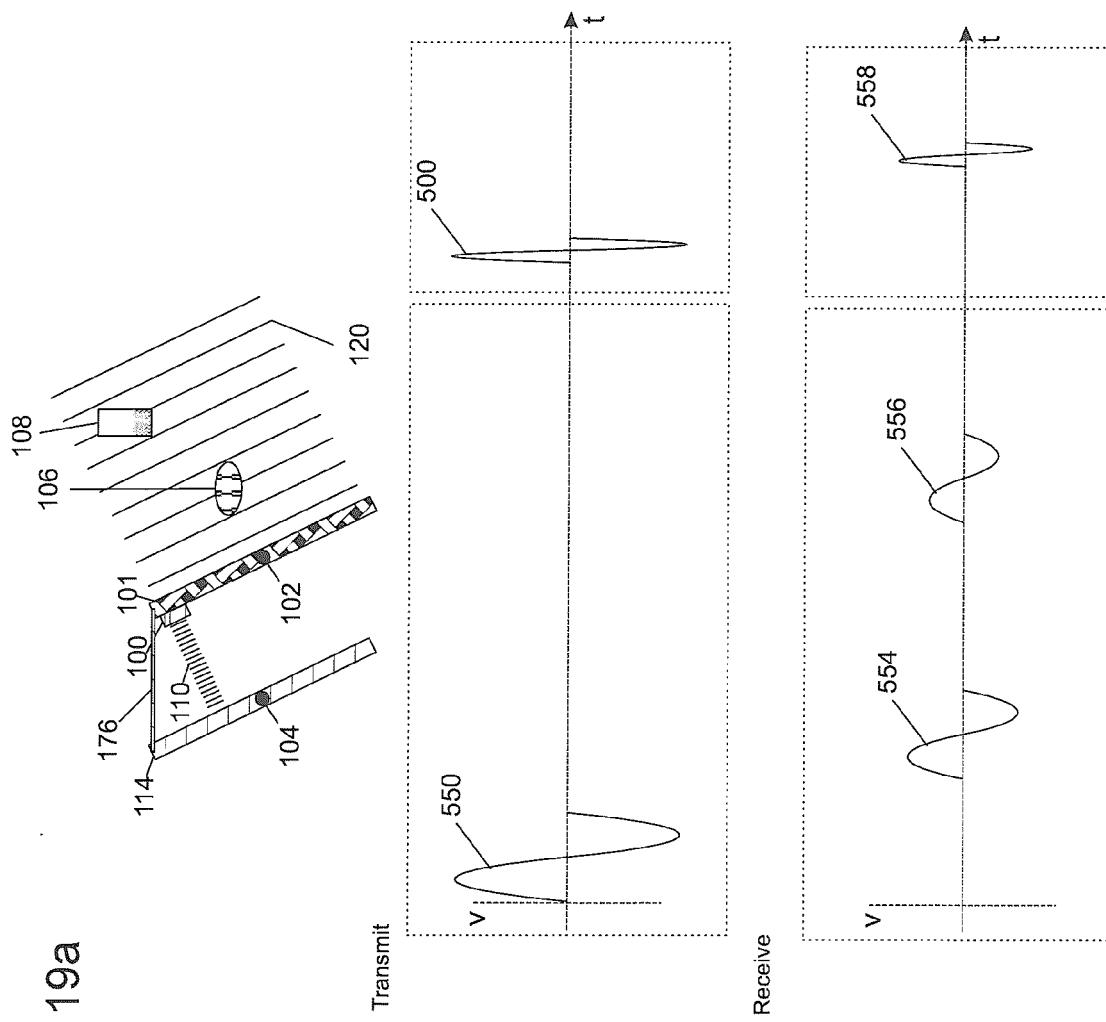


FIG. 19b

FIG. 19c

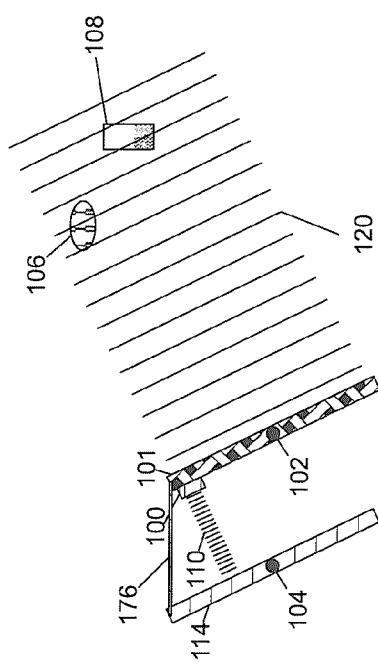


FIG. 19d

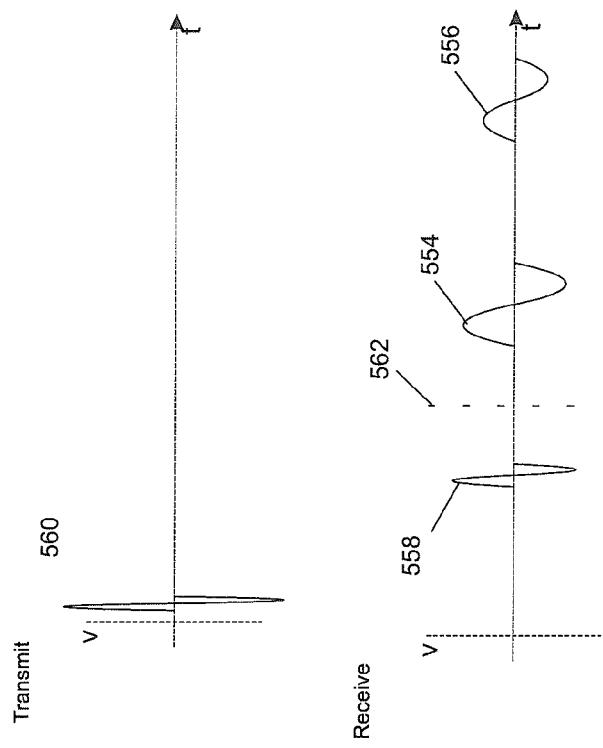


FIG. 19e

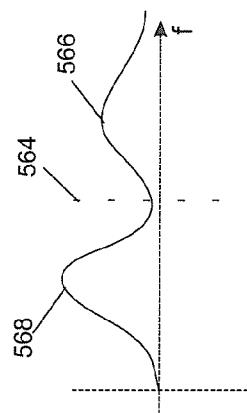


FIG. 19f

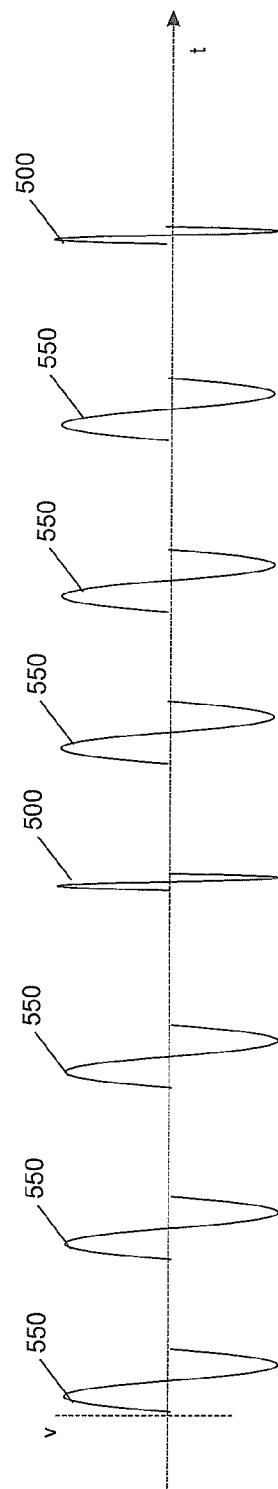


FIG. 19g

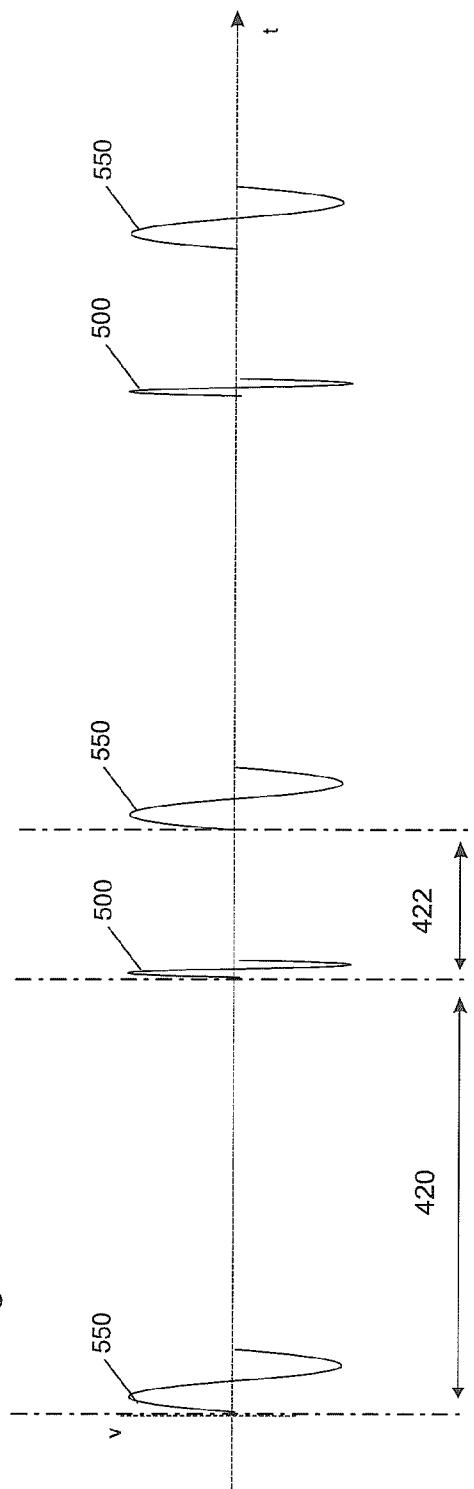


FIG. 20a

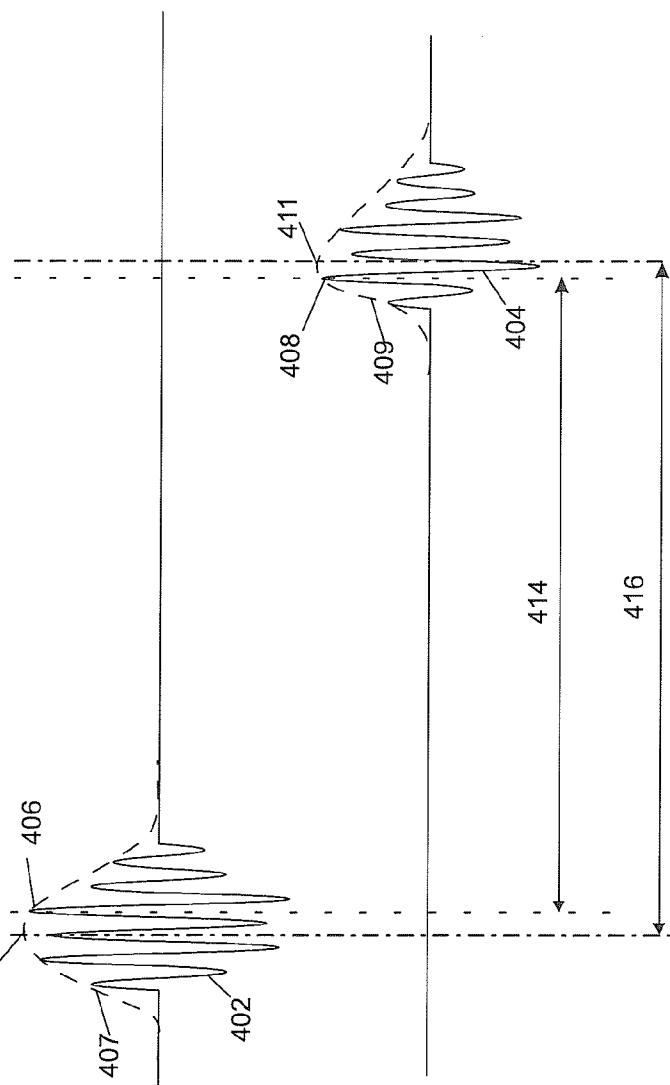


FIG. 20b

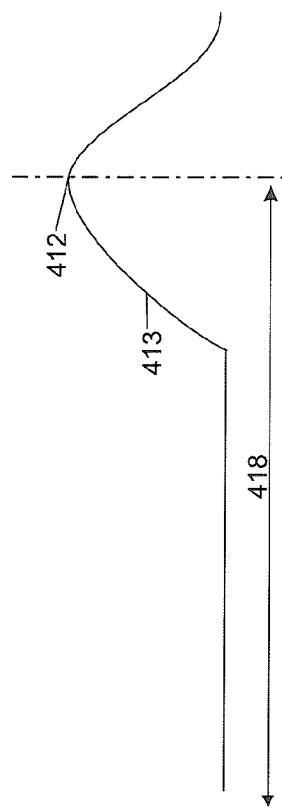
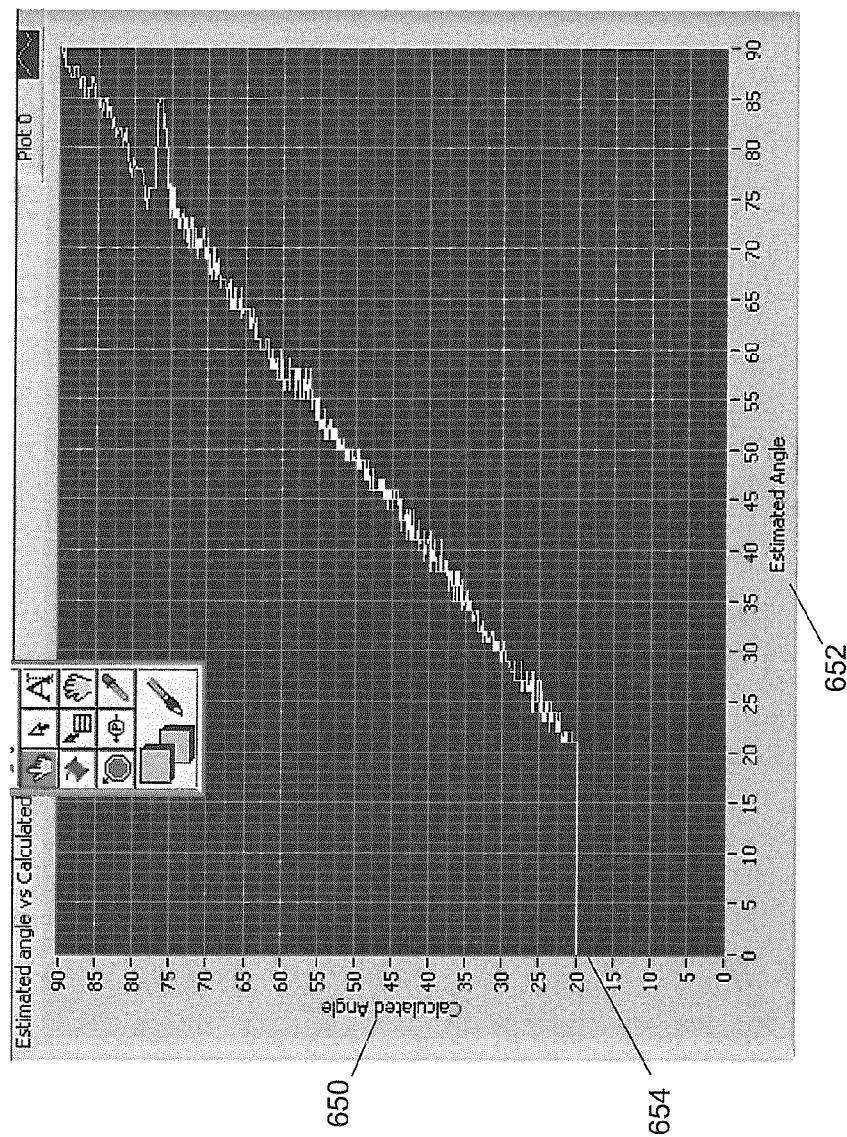


FIG. 21



REFERENCES CITED IN THE DESCRIPTION

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- US 20080177138 A [0025] [0037]

专利名称(译)	具有超声波换能器的超声波探头可在公共电气通道上寻址		
公开(公告)号	EP2671093B1	公开(公告)日	2019-01-16
申请号	EP2012742001	申请日	2012-01-31
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IPC分类号	G01S15/89 A61B8/00 F16F1/14 G01D5/48 G01S7/52 G01S7/527 G01N21/64 G01N21/65 G01N29/14 G10K11/00		
CPC分类号	A61B8/12 A61B8/14 A61B8/445 A61B8/4466 B06B1/06 G10K11/352		
代理机构(译)	丹麦美国律师协会		
优先权	61/437758 2011-01-31 US		
其他公开文献	EP2671093A4 EP2671093A1		
外部链接	Espacenet		

摘要(译)

提供了用于电寻址多个超声换能器的方法和装置，所述超声换能器连接到公共电通道并容纳在成像探头内。成像探头可以包括成像超声换能器和用于控制发射的成像光束的方向的可移动元件，以及角度感测超声换能器，其中角度感测超声换能器被配置用于确定超声成像束的方向。角度感测换能器可以被配置为将角度感测超声波束引向声学反射基板并通过检测从声学反射基板反射的反射超声波束来提供信号，其中声学反射基板相对于可移动元件定位。可移动元件的运动产生信号的变化。

