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(54) ULTRASONIC SYNTHETIC TRANSMIT FOCUSING WITH A MULTILINE BEAMFORMER

SYNTHETISCHE ULTRASCHALLÜBERTRAGUNGSFOKUSSIERUNG MIT MEHRZEILIGEM STRAHLFORMER

ÉMISSION SYNTHÉTIQUE ULTRASONIQUE SE FOCALISANT SUR UN FORMEUR DE FAISCEAUX MULTILIGNES

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(56) References cited:
US-A- 4 644 795 US-A- 5 793 701
US-A1- 2002 144 549 US-B1- 6 589 177
US-B2- 6 482 157 US-B2- 6 482 157

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Description

[0001] This invention relates to medical diagnostic ultrasound systems and, in particular, to ultrasound systems which extend the focal region using a multiline receive beamformer.

[0002] The principles of synthetic focusing, by which an ultrasound image is focused at every point in the image field, have been the subject of considerable investigation. For instance, US patent 4,604,697 (Luthra et al.) describes a synthetic focus technique in which an ultrasound pulse is sequentially transmitted from each element of an ultrasonic transducer array. The echo signals received from each transmission is received by all of the elements of the array and are stored. After all of the signals have been received a focused echo signal can be formed at each point in the image field from the knowledge of the location of each transducer element relative to each point in the image and the time of flight of an ultrasound signal to and from each point. The appropriate received signals are combined to form a coherent echo signal for each point in the image. The selection of the stored data values used to form each point provides the beamformation for each point in the image. While this method will produce a focused signal at every point in the image field, it has several drawbacks. One is that the r.f. signals from the entire image field must be stored for processing. This requires a significant amount of information storage. A second drawback is that a significant amount of processing is required to select and weight the data for each point in the image, then combine the appropriately weighted data to compute the image data points. A third drawback is that this approach is effective for only a shallow penetration depth, since the energy transmitted by a single transducer element is limited.

[0003] A specific application which employs the basic principles of synthetic focusing is the traditional delay-and-sum receive beamformer, in which the delays applied to the signals from each receiving element are the equivalent of data selection in the synthetic focus technique. The traditional beamformer is a limited application of these principles as it transmits a transmit beam focused at a specific focal region and dynamically focuses echoes only along this single transmit beam. Multiple transmissions are thus required to scan the entire image field. A resulting efficiency is that data does not need to be stored for all transmissions to every point in the image; the data received from a transmission is immediately processed to form coherent echo signals along the beam direction. A limitation is that each received beam is focused on transmit to only the selected focal region. But the signal-to-noise ratio at greater depths is improved because multiple transducer elements are actuated to transmit a beam, enabling a reasonable penetration to be obtained.

[0004] US patent 6,231,511 (Bae et al.) and a subsequent paper entitled "A Study of Synthetic-Aperture Imaging with Virtual Source Elements in B-Mode Ultrasound Imaging Systems" by Bae et al., IEEE Trans. UFFC, vol. 47, no. 6 (2000) at 1510 et seq. propose to combine aspects of the standard focused beamformer and synthetic focusing to improve lateral resolution outside of the conventional focal region and thus achieve the effect of transmit focusing at all points in the image field. This approach is premised upon the assumption of a "virtual source element" at the focal point of a standard transmitted beam which radiates energy both outward and inward from this "virtual source." Following transmission of a standard transmit focused beam, energy is received by the transducer elements of the receive aperture and stored. After the entire image field has been scanned, an echo signal at each point is computed from the signals received by elements of each virtual source field which encompassed the point in the field. Image points at the focal point will be imaged from only one beam, as the virtual source model is an hourglass-shaped field about the transmit focal point, but points further removed in depth from the focal point are computed from the received signals of many scanlines. The result is said to be an image which shows improved lateral resolution at points outward and inward from the transmit focal point. But like the basic synthetic aperture approach described above, a significant amount of data must be stored for processing, the r.f. signals from every element in each receive aperture. In addition the resultant image is said to appear darker around the focal point, since only one transmission and reception contributes to this image point and its resolution, whereas multiple transmissions and receptions contribute to points removed from the transmit focal point. Accordingly it is desirable to effect transmit focusing over at least a significant portion of an image but without the need to store vast amounts of r.f. data.

[0005] US 5,793,701 A discloses a method and apparatus for imaging an object using a transducer array for transmitting one or more beams that are steered and/or translated to transmit scan lines for multiple excitation events so as to scan a field of view of the object, for sensing received signals reflected from the object after each excitation event on one or more receive beams on receive scan lines, and for transducing those sensed received signals into corresponding electrical signals. Said method and apparatus is additionally for acquiring and storing coherent samples retaining both phase and amplitude information of those electrical signals obtained on the receive scan lines throughout at least a portion of the field of view, and for combining stored coherent samples associated with distinct receive beams to synthesize new coherent image samples aligned on synthetic scan lines which are distinct from any one of (1) receive scan lines on which a signal was sensed, (2) transmit scan lines on which a signal was directed, or (3) transmit scan lines and receive scan lines.

[0006] The above-mentioned problems are overcome by an ultrasonic diagnostic imaging system according to independent claim 1 and a method for producing an ultrasound image with an extended focal range according to independent claim 13.

[0007] In accordance with the principles of the present invention, a diagnostic ultrasound system and method are described which effect transmit focus over a significant depth of field without the need to store r.f. signal data. An ultrasound beam is transmitted which insonifies at least portions of multiple scanline locations and receive beams are concurrently processed along the multiple scanlines, e.g., in parallel or by time multiplexing. A succession of such transmissions produces multiple scanlines related to a common scanline location. Preferably, the related scanlines are concentrically aligned. The related scanline data is beamformed to produce echo data which is effectively transmit focused over a significant depth of field. In an example described below, an ultrasound system receives the simultaneous beams with a multiline beamformer. An implementation of the present invention can improve the frame rate of ultrasound imaging by reducing the need to resort to multizone focusing in some clinical applications.

[0008] In the drawings:

FIGURES 1a-1c illustrate beam profiles of a three-beam example of the present invention.

FIGURES 2a-2d illustrate beam profiles of a six-beam example of the present invention.

FIGURES 3a-3d illustrate a four-beam example of the present invention in which the first four beam patterns are offset for clarity of illustration.

FIGURES 4a-4d illustrate a continuation of the four-beam example of FIGURE 3 showing the alignment of the receive beams.

FIGURE 5 illustrates in block diagram form an ultrasound system constructed in accordance with the principles of the present invention.

FIGURES 6a and 6b illustrate the delay and weighting characteristics of two different beams of the four-beam example of the present invention.

FIGURE 7 illustrates in block diagram form an ultrasound system which adaptively responds to motion to adjust the number of multilines being combined in an implementation of the present invention.

[0009] Referring first to FIGURES 1a-1c, overlapping beam profiles are shown for the transmission of three transmit beams followed in each case by the reception of three beams from each transmit beam. FIGURE 1a shows the transmit beam profile 10 at a constant level below the intensity peak at the center of the beam, transmitted by and extending from a transducer array 8 that transmitted the beam. The transmit beam profile level is chosen by the designer and may be 3 dB, 6 dB, 20 dB, or some other level below the maximum intensity at the center of the beam. The beam profile is seen to be focused about a focal point 12 at the narrowest width of the beam profile by conventional transmit focusing. An orthogonal view of the beam 20 is shown below the transducer array 8 which is seen to comprise a center lobe 20a and side lobes on either side of the main lobe 20a. The transmitted beam reaches its tightest focus at the focal region 12 and diverges thereafter. In other implementations a diverging transmit beam may be used. Focusing at a considerable depth has also been found to be effective.

[0010] The transmit beam 10, 20 is transmitted with a width that encompasses multiple receive lines 14, 16, and 18. Generally a wider beam is produced by transmitting from a smaller transmit aperture. That is, a lesser number of elements of the array 8 are actuated to transmit the beam than the total number of elements across the array. Following transmission echoes are received and focused along three receive line locations 14, 16 and 18. As discussed below, the echoes received by the transducer elements of the receive aperture are delayed and summed in three different ways to form multiple lines at different line locations 14, 16, and 18 in response to one transmit beam. In this example receive line 16 is received down the center of the transmit beam 10, 20 and receive lines 14 and 18 are laterally steered and focused to be received on either side of the center line. In this example only the near field and far field portions of the outer lines 14 and 18 are within the transmit beam profile 10. In these regions the outer lines 14 and 18 are received from transmit energy on either side of the center line position thereby sampling targets in the image field on both sides of the center line position, thereby efficiently using the laterally spread energy of the transmit beam in the near and far fields for image reception and resolution.

[0011] In FIGURE 1b a second beam has been transmitted by shifting the transmit aperture to the right by the spacing of one receive line. The second transmit beam has the same beam profile as the first transmit beam and is outlined by beam profile curves 10'. As in the case of the first beam, three receive lines are simultaneously received and beamformed in response to the second transmission at receive line locations 16', 18' and 22. As a result, receive line 16' is aligned with receive line 16 from the first transmission, receive line 18' is aligned with receive line 18 from the first transmission and receive line 22 is located to the right of the center line 18' of the second transmission. Like the first set of receive lines, the second set of receive multilines 16', 18', and 22 is saved for subsequent processing.

[0012] In FIGURE 1c a third beam has been transmitted from a center aperture location which is again shifted to the right by one receive line. This transmit beam is outlined by beam profile 10" and the transmission is followed by the simultaneous reception of three receive lines 18", 22' and 24. These three receive lines, like the previous receive lines, are wholly or partially within the beam profile of their transmit beam with the same spacing as the lines of the preceding beams. As a result, receive line 18" is axially aligned with receive line 18' of the second transmission and receive line

18 of the first transmission, and receive line 22' is axially aligned with receive line 22 of the second transmission. The targets in the path of receive lines 18, 18' and 18" have now been sampled by three receive lines, each by a respectively different transmit beam. These co-aligned beams are combined as described below to produce a line of image data along the line which are focused over a greater depth of field than is the case of any individual line, creating an extended transmit focus effect. The focusing will be effective over a greater depth of field as the echo energy from three beam transmissions is combined to produce the resultant image data.

[0013] Transmission and reception continues across the image field in this manner until the full image field has been scanned. Each time the maximum number of receive lines for a given line location has been acquired, three in this example, the receive lines are processed together to produce a line of image data at that location. There is thus no need to store pre-summed r.f. data from any transmission as the received r.f. signals are beamformed into multiple lines as they are received, and there is only a limited need to store previous lines at a line location until all of the receive lines at the location have been acquired, at which time they can be processed and the line storage freed up for storage of subsequent lines.

[0014] FIGURES 2a-2d give another example of the present invention in which the transmit beam profile 30 includes all or portions of receive lines at six receive line locations, identified at 31-36 in FIGURE 2a. In this example, unlike the first, there is no receive line at the center of the transmit beam. Instead, central receive lines 33 and 34 are spaced one-half of a receive line spacing on either side of the center of the transmit beam. The outer receive lines 32 and 35 are within the beam profile 30 in the near and far fields, and only near field portions of the outermost receive lines 31 and 36 are within the transmit beam profile. It may be decided not to use these near field line portions 31 and 36 in image data formation as explained below.

[0015] The next transmit beam is transmitted to the right of the first transmit beam by one receive line spacing as shown by the profile 30' of the second transmit beam in FIGURE 2b. Six receive lines are again received and beamformed simultaneously at receive line locations 32', 33', 34', 35', 36' and 37. The first five of these receive lines are seen to be aligned with receive lines 32, 33, 34, 35 and 36 of the first transmit beam, thus providing a second receive line for processing at each of these line locations. FIGURE 2c shows the results following transmission of a third transmit beam and reception of six receive lines within that beam profile 30". There now have been all or parts of three receive lines received at line locations 33", 34", 35" and 36", two receive lines at location 37', and a portion of one receive line at location 38. Following a fourth transmission, indicated by beam profile 30''' in FIGURE 2d, there have been all or portions of four receive lines received at line locations 34"', 35''' and 36''', three receive lines received at line location 37'', two receive lines received at line location 38' and a portion of one receive line received at line location 39. It can be seen that, when scanning continues in this manner, there will be all or portions of six receive lines received at the line locations across most of the aperture, except at the extremes where fewer lines will have been received as shown in this example. The greater number of samplings of each receive line location results in better effective transmit focusing when the receive line data is combined to form the image data.

[0016] Higher numbers of simultaneously received lines may be used, such as eight, twelve or sixteen spaced apart, simultaneously received lines, for which a lower F number on transmit should be used to insonify the greater expanse of receive line locations.

[0017] FIGURES 3 and 4 illustrate another example of the present invention using four receive lines from every transmit beam. In these drawings the successive beam and receive line groups are not overlapping but are vertically aligned for clarity of illustration. Each transmit beam 40-1, 40-2, 40-3, etc. is indicated by a dashed arrow pointing downward, and the receive lines from each transmit beam are shown as solid line arrows on either side of the respective transmit beam. FIGURES 3a-3d illustrate the first four transmit-receive sequences, with the transmit beam 40-n being shifted to the right by one receive line spacing for each successive transmit interval. At the end of this transmit-receive sequence it is seen that four receive lines have been received which are aligned with receive line 44: receive line 44-1 from the second beam, receive line 44-2 from the third beam, and receive line 44-3 from the fourth beam. These four receive lines are combined to produce a line of image data at the location of these receive lines in the image field.

[0018] FIGURES 4a-4d show a continuation of the previous transmit-receive sequence with four more transmit-receive intervals of four simultaneously received lines for each transmit beam. The next four transmit beams are identified as 40-5, 40-6, 40-7, and 40-8 in these drawings. As these drawings illustrate, there now have been four receive lines received at line locations 44, 45, 46, 47 and 48. After the four receive lines at each of these locations has been received the four lines can be combined to form one line of image data and the stored receive lines deleted so that subsequent lines can be stored in the same storage locations. Each time another fourth line of a group of four aligned lines has been received, the four lines of the group can be combined to form the line of image data at that location and the storage used for subsequent lines. The sequence continues in this manner, receiving four receive lines for each transmitted beam across the image field so that four receive lines may be combined at each line location over all but the lateral extremities of the image field.

[0019] FIGURE 5 illustrates in block diagram form an ultrasonic imaging system constructed in accordance with the principles of the present invention. An ultrasonic probe 102 includes a transducer array 104 of transducer elements.

Selected groups of the transducer elements are actuated at respectively delayed times by the transmit beamformer 106 to transmit beams focused at selected focal regions in the desired directions and from the desired origin(s) along the array. The transmit beamformer is coupled to the transducer elements by a transmit/receive switch 108 which may comprise a crosspoint switch that protects the receiver inputs from the high voltage transmit pulses applied. The echoes received by each transducer element of the array 104 in response to each transmit beam are applied to the inputs of multiline processors 110a-110n. Each multiline processor comprises a receive beamformer which applies its own set of delays and, if desired, apodization weights to weight the received echoes from the array elements to form a differently steered receive beam from the same transmit beam. Suitable multiline beamformers for the multiline processors 110a-110n may be found, for instance, in US Pat. 6,695,783 (Henderson et al.) and US Pat. 5,318,033 (Savord). The outputs of the multiline processors 110a-110n are coupled to a line store 112 which stores the received multilines at least until all of the multilines needed to form a line of display data have been acquired. The group of multilines used to form a particular line of display data are applied to respective ones of multipliers 116a-116n to produce the display data for the corresponding line location. The echo data from each line may, if desired be weighted by apodization weights 114a-114n. In general, these weights will weight each line as a function of its round-trip impulse response. A suitable weighting algorithm can be derived by letting the term *amplitude(x,z)* be theinsonification amplitude of a point at location (x,z) in the image field by the transmit wave-front, the azimuth position x=0 corresponding to the center axis of the transmit beam. Let X be the azimuth of the received multiline with respect to the transmit beam axis. The weight applied to this received multiline to form a point of the image at depth Z is:

$$Weight(X,Z) = amplitude(X,Z)$$

For determination of an appropriate delay characteristic, let *propagation_time(x,z)* be the propagation time needed by the transmit wavefront to reach a point at location (x,z), the azimuth x=0 corresponding again to the center axis of the transmit beam. Let X be the azimuth of the receive line with respect to the transmit beam axis. The delay applied to this received multiline to form a point of the image at depth Z is:

$$Delay(X,Z) = propagation_time(X,Z) - propagation_time(0,Z)$$

where *propagation_time(0,Z)* is the time to reach a point at the same depth but on-axis.

[0020] The functions *amplitude(X,Z)* and *propagation_time(X,Z)* may, for example, be obtained from a simulation of the transmit field. An appropriate way to compute the propagation time is to use the phase delay of the field from monochromatic simulation at several frequencies. The amplitude may be computed by averaging the amplitude of the field at several frequencies. In addition, a depth-dependent normalization can be applied to the weights. This multiplies all the weights at a given depth by a common factor. For example, the normalization can be chosen so that speckle regions have uniform brightness with depth. By varying the weights as a function of depth, it is possible to vary the size and shape (apodization) of the aperture dynamically with depth.

[0021] The amplitude and propagation time do not need to be derived from a simulation of the exact transmit characteristics used in the system. The designer may choose to use a different aperture size or a different apodization for example.

[0022] The echoes from each line are weighted by the multipliers 116a-116n and delayed by delay lines 118a-118n. In general, these delays will be related to the location of the transmit beam center to the receive line location as shown above. The delays are used to equalize the phase shift variance that exists from line to line for the multilines with differing transmit-receive beam location combinations, so that signal cancellation will not be caused by phase differences of the combined signals.

[0023] It will be appreciated that in a digital system the delay lines may be effected by storing the weighted multiline echo data in memory and reading the data out at later times which effect the necessary delay. Shift registers of differing lengths and clock signals may also be used to effect a digital delay, or an interpolating beamformer such as that described in the aforementioned US Pat. 6,695,783 may be used. The delayed signals are combined by a summer 120 and the resultant signals are coupled to an image processor 122. The image processor may perform scan conversion or other processing to improve the displayed image. The resultant image is displayed on an image display 124.

[0024] In the system of FIGURE 5 the delay lines 118 and summer 120 effect a refocusing of the signals received from the several receive multilines which are co-aligned in a given direction. The refocusing adjusts for the phase differences resulting from the use of different transmit beam locations for each multiline, preventing undesired phase cancellation in the combined signals. The weights 114 weight the contributions of the multilines in relation to the proximity of the transmit beam to the multiline location, giving higher weight to receive beams with higher signal-to-noise ratios.

This results in an extended depth of field along each receive line and an enhanced penetration (improved signal-to-noise ratio) due to the combination of multiple samplings in each receive line direction.

[0025] In the example of FIGURES 4a-4d it is seen that each received multiline is only used once in combination with other co-aligned multilines. This means that an implementation of the present invention does not require the second set of weights 114 multipliers 116 and delays 118, because these weighting and delay effects can be implemented with the weights and delays of the multiline processors 110, which can focus the multiline in the proper receive direction and account for phase and transmit beam variation with respect to the multilines with which it is to be combined, all in one process step. After all the multilines for a given line location have been received they are simply summed to provide the display line data. Alternatively each received multiline for a given line location is stored in a line accumulator for that line. Each subsequently received multiline at that line location is added to the contents of the accumulator until the full complement of multilines at that location has been combined in the accumulator. The accumulator contents are then forwarded to the image processor, freeing the accumulator for use for another line location.

[0026] FIGURES 6a and 6b illustrate examples of the weighting and delay characteristics that may be used in combining the received multilines for a given display line location. FIGURE 6a illustrates example weighting and delay characteristics for a received multiline that is relatively distant from the transmit beam center such as received multiline 33' of FIGURE 2b. The received multiline 33' is shown extending in the z direction from the face of the transducer array at z=0 to the maximum scan depth on the right side of the drawing. The center of the multiline is drawn as dotted where that portion of the multiline 33' is outside of the selected beam profile 30' and its response is below that which the designer has deemed to be acceptable. The weighting characteristic 82 thus weights this multiline with a weight which is at a minimum where it is beyond the beam profile and at nonzero levels where the multiline is to be used for refocusing. In other implementations the weighting characteristic 82 may drop to zero in the near field. This is because the echoes may be too close to or behind the array after the necessary delay has been applied and thus not susceptible to accurate reception. Thus the multilines from laterally distant multilines are not used in the multiline combination in the very near field.

[0027] The phase characteristic 84 is seen to cross through a zero phase adjustment at the focal point of the transmit beam, staying nearly constant in the near field and gradually decreasing in the far field.

[0028] FIGURE 6b illustrates exemplary weighting and delay characteristics for a received multiline 33 that is closer to the center of its transmit beam. Due to this closer proximity the multiline is given greater overall weighting in the combination as shown by the weighting characteristic 86. The weighting increases in the vicinity of the focal region to balance the falloff of the weighting of the more remote multilines such as 33' in this region. The phase adjustment characteristic 88 is drawn as a straight line because the delay characteristic 84 for the more laterally remote multiline is calculated from the phase of the more central multiline 33. In this example the multiline 33 is used for refocusing over the full image depth, although in a given implementation the designer may elect to use the echoes of a single line from a transmit beam in close proximity to the line location in the very near field.

[0029] An implementation of the present invention can be used with a variety of receive functions. For instance an implementation can operate on signals from focused sub-apertures. In another variation, instead of forming receive beams *per se*, a limited number of orthogonal functions such as Fourier components can be used. It is then possible to combine the different transmits in Fourier space.

The signals being combined do not correspond exactly to received image lines. Thereafter receive beams are formed by combining the Fourier components or sub-apertures. Various combinations of several beams and functions derived from a beam by a change of apodization are also within the scope of the present invention. In other implementations a small number of received multilines can be increased by interpolating additional intermediate multilines, then performing the inventive processing with the increased number of multilines.

[0030] FIGURE 7 illustrates a variation of the ultrasound system of FIGURE 5 in which the effects of motion are addressed. The example shown in FIGURE 5 combines the r.f. signals received from a number of co-aligned multilines of different transmit-receive intervals. Since it is r.f. signals and not detected signal envelopes which are being combined, it is important that there be little motion in the image over the period that the multilines which are to be combined are received. Significant motion, either of materials in the image field or of the probe with respect to the image field, can cause r.f. signal differences which result in cancellation rather than the desired signal reinforcement when the signals from the different multilines are combined. This problem is more acute with longer acquisition intervals during which greater numbers of multilines are acquired for combining. The example of FIGURE 7 addresses this problem by detecting relative image motion and adjusting the multiline order in response to the presence of motion. A motion detector 130 receives consecutive image frames from the image processor 122 and compares the image content for differences which are indicative of motion. A suitable technique for doing this is a correlation technique which correlates the image pixel values in the same area or areas of consecutive images. This can be done by calculating the zero-lag normalized cross-correlation between the data of the two images. If the correlation factor is high (i.e., the images are nearly identical), a larger number of multilines, requiring a greater number of transmit-receive intervals, are used to improve the depth of field. When the correlation factor is low (the images are different), which can be due to motion within the image field or by the probe, a lesser number of multilines are combined. A suitable correlation technique is the minimum sum of absolute

differences (MSAD) technique described in US Pat. 6,126,598 (Entrekin et al.). As described in this patent, the data which undergoes MSAD processing for motion detection can be areas of images or reference lines transmitted during or between image frames. Doppler techniques can also be used to detect motion as described in US Pat. 5,127,409 (Daigle).

[0031] The result of motion detection is coupled to a multiline controller 132 which adjusts the transmission and reception of multilines as a function of motion, with lower order multiline used when motion is present. The adjustments made in this example are in control of the transmit beamformer to transmit a larger F number beam which laterally encompasses fewer multilines when motion is present so that the multilines which are combined span a shorter period of transmit times. Smaller transmit apertures can be used with broader focal regions which are more uniform over a larger range of depths, requiring fewer transmit beams to cover the field of view. On reception the multiline controller 132 controls the number of multiline processors employed, with fewer needed for the reception of fewer multilines in the presence of motion. The multiline controller 132 is also coupled to the line store 112 to command the refocusing of the fewer number of multilines by the weights 114, delay lines 118 and summer 120 when motion is present. The result of these adjustments are that a shorter time is needed to acquire the multilines which are to be combined, the shorter time period being less affected by motion than would a longer acquisition interval. Correspondingly, when the motion detector detects a stationary image field when motional effects are low, the multiline order is increased by the multiline controller. An exemplary adjustment range is to use 16x multiline (receiving sixteen multilines in response to a transmit beam and combining multilines from sixteen transmit beams) when the image field is stationary, and decreasing the multiline order to 8x, 4x, 2x and 1x (single line transmit and receive) as the amount of motion increases. For instance, when the probe is being moved over the body of a subject in a search for certain anatomy or a good viewing perspective, standard single line imaging would be used. The multiline order can also be automatically changed as a function of the imaging mode of the ultrasound system. For instance, when the system is changed from B mode imaging to Doppler imaging, multiline acquisition can be discontinued by the multiline controller. The degree of multiline can be automatically set during imaging by the multiline controller, and/or the user can be provided a manual control to set the degree of multiline.

[0032] Variations of the examples above will readily occur to those skilled in the art and are within the scope of the present invention. For example, instead of transmitting along successive line locations, transmission can skip lines (multiplex) between multiline transmission. Transmission can be done along every other line position, every fourth line position, or other intervals of multi-line spacing, thus reducing the number of transmit events needed to form the image and increasing the acquisition rate. This is also a way to reduce motion artifacts. Receiving multilines at more widely spaced line intervals with a fewer number of transmit beams is another way to address the problem of motion. This approach can be augmented with interpolated lines as mentioned above to increase the number of lines which are combined. This will also increase the depth of field improvement for a given number of multilines. The sampling used is generally a function of the F number of the transmit aperture, which determines the Nyquist sampling requirement. Scanning does not have to be done sequentially across the image; other transmission sequences can be used, which will have different responses in the presence of motion. While the examples above are shown with apodization, it is not necessary to apodize on transmission, reception, or multiline combination. It is not necessary that the multilines to be combined all be precisely axially aligned. Multilines which are to be combined can be offset laterally from each other, effecting an interpolation when the multilines are combined. The principles of the present invention are also applicable to three dimensional imaging by performing the processing in both the elevation and azimuth dimensions, and to phased array (sector scan) imaging as well as linear array (orthogonal scan) imaging and by use of curved arrays.

Claims

1. An ultrasonic diagnostic imaging system comprising:

a probe (102) including an array of transducer elements (8, 104);
 a transmit beamformer (106), coupled to the array of transducer elements (8, 104), and operable to transmit a beam (10, 20, 30) from a plurality of transmit beam locations, each beam exhibiting a focal region and encompassing a plurality of laterally spaced line positions;
 a multiline receive beamformer (110a-110n), coupled to the array of transducer elements (8, 104), which is operable to produce a plurality of receive lines at the line positions in response to one transmit beam (10, 20, 30) at each of different beam locations;
 a multiline combining circuit (114a-114n; 116a-116n; 118a-118n; 120), responsive to a plurality of receive lines which relate to a common line position produced by the multiline receive beamformer (110a-110n) in response to a plurality of transmit beams (10, 20, 30), said multiline combining circuit being operable to combine the plurality of receive lines at the common line position to produce image data; and
 a display (124) which produces an image utilizing the image data; **characterized in that**

the multiline combining circuit (114a-114n; 116a-116n; 118a-118n; 120) includes a plurality of delays, wherein a delay for each receive line is related to the position of the receive line at the respective line position relative to the center of its transmit beam in order to equalize the phase shift variance among the receive lines from different transmit beams at the respective line position.

2. The ultrasonic diagnostic imaging system of Claim 1, wherein the multiline combining circuit includes a summer (120) which is operable to combine data from different multilines.
3. The ultrasonic diagnostic imaging system of Claim 2, wherein the multiline combining circuit further includes a plurality of weighting circuits (114a-114n) which are operable to weight multiline data.
4. The ultrasonic diagnostic imaging system of Claim 1, wherein the probe (102) comprises a linear array probe.
5. The ultrasonic diagnostic imaging system of Claim 1, wherein the probe (102) comprises a phased array probe.
6. The ultrasonic diagnostic imaging system of Claim 1, wherein the transmit beamformer (106) is further variable to transmit a beam from a selected transmit aperture.
7. The ultrasonic diagnostic imaging system of Claim 6, wherein the transmit beamformer (106) is operable to transmit a sequence of beams from a sequence of different apertures along the transducer array (8, 104).
8. The ultrasonic diagnostic imaging system of Claim 7, wherein the transmit beamformer (106) is further operable to transmit a sequence of beams from a sequence of different apertures selected such that at least some of the laterally spaced line positions of one beam are aligned with at least some of the laterally spaced line positions of another beam.
9. The ultrasonic diagnostic imaging system of Claim 8, wherein the transmit beamformer (106) is further operable such that at least some of the laterally spaced line positions of one beam are coaxially aligned with at least some of the laterally spaced line positions of another beam.
10. The ultrasonic diagnostic imaging system of Claim 1, wherein the multiline receive beamformer (110a-110n) includes a plurality of multiline processors, each of which applies a set of delays to signals received from a plurality of transducer elements to focus a receive multiline in a selected line direction.
11. The ultrasonic diagnostic imaging system of Claim 10, wherein the multiline receive beamformer (110a-110n) exhibits a variable multiline order.
12. The ultrasonic diagnostic imaging system of Claim 1, further including a line store coupled to the multiline receive beamformer (110a-110n) and operable to store receive lines produced in response to a plurality of transmit beams.
13. A method for producing an ultrasound image with an extended focal range, comprising:
 - transmitting a plurality of transmit beams (10, 20, 30) from an array transducer (8, 104), each transmit beam being centered at a different position along the array (8, 104) and each transmit beam (10, 20, 30) encompassing a plurality of laterally spaced line positions which are spatially related to laterally spaced line positions of another beam;
 - receiving echo signals with the array transducer (8, 104);
 - concurrently processing the echo signals received in response to one transmit beam (10, 20, 30) to produce a plurality of receive lines of echo signals at the laterally spaced line positions of the beam;
 - repeating the concurrently processing for additional transmit beams (10, 20, 30);
 - combining echo signals of receive lines from different transmit beams (10, 20, 30) which relate to a common line position to produce image data; and
 - producing an image using the image data;
 - characterized in** the step of equalizing the phase shift variance among all receive lines at a common receive line position resulting from transmit beams of different transmit beam locations by applying delays which are related to the location of each receive line at the common receive line position relative to the center of its transmit beam.
14. The method of Claim 13, further comprising relatively weighting the signals of receive lines from different transmit

beams prior to combining.

Patentansprüche

1. System zur diagnostischen Ultraschallbildgebung, das Folgendes umfasst:

eine Sonde (102) mit einem Array von Wandlerelementen (8, 104);
 einen Sendestrahlformer (106), der mit dem Array von Wandlerelementen (8, 104) gekoppelt ist und betriebsfähig ist, um ein Strahlenbündel (10, 20, 30) von einer Vielzahl von Sendestrahlenbündelorten aus zu senden, wobei jedes Strahlenbündel eine Fokusregion aufweist und eine Vielzahl von lateral beabstandeten Linienpositionen umfasst;
 einen Mehrlinien-Empfangsstrahlformer (110a-110n), der mit dem Array von Wandlerelementen (8, 104) gekoppelt ist und betriebsfähig ist, um eine Vielzahl von Empfangslinien an den Linienpositionen in Reaktion auf ein Sendestrahlenbündel (10, 20, 30) an jeder von verschiedenen Strahlenbündelorten zu erzeugen;
 eine Mehrlinien-Kombinierschaltung (114a-114n; 116a-116n; 118a-118n; 120), reagierend auf eine Vielzahl von Empfangslinien, die sich auf eine gemeinsame Linienposition beziehen, erzeugt durch den Mehrlinien-Empfangsstrahlformer (110a-110n) in Reaktion auf eine Vielzahl von Sendestrahlenbündeln (10, 20, 30), wobei die genannte Mehrlinien-Kombinierschaltung betriebsfähig ist, um die Vielzahl von Empfangslinien an der gemeinsamen Linienposition zu kombinieren, um Bilddaten zu erzeugen; und
 eine Anzeige (124), die unter Verwendung der Bilddaten ein Bild erzeugt; **dadurch gekennzeichnet, dass** die Mehrlinien-Kombinierschaltung (114a-114n; 116a-116n; 118a-118n; 120) eine Vielzahl von Verzögerungen umfasst, wobei sich eine Verzögerung für jede Empfangslinie auf die Position der Empfangslinie an der jeweiligen Linienposition relativ zu der Mitte ihres Sendestrahlenbündels bezieht, um die Phasenverschiebungsvarianz unter den Empfangslinien aus verschiedenen Sendestrahlenbündeln bei der jeweiligen Linienposition auszugleichen.

2. System zur diagnostischen Ultraschallbildgebung nach Anspruch 1, wobei die Mehrlinien-Kombinierschaltung einen Summierer (120) umfasst, der betriebsfähig ist, um Daten von verschiedenen Mehrlinien zu kombinieren.

3. System zur diagnostischen Ultraschallbildgebung nach Anspruch 2, wobei die Mehrlinien-Kombinierschaltung weiterhin eine Vielzahl von Gewichtungsschaltungen (114a-114n) umfasst, die betriebsfähig sind, um Mehrliniendaten zu gewichten.

4. System zur diagnostischen Ultraschallbildgebung nach Anspruch 1, wobei die Sonde (102) eine Lineararray-Sonde umfasst.

5. System zur diagnostischen Ultraschallbildgebung nach Anspruch 1, wobei die Sonde (102) eine Phased-Array-Sonde umfasst.

6. System zur diagnostischen Ultraschallbildgebung nach Anspruch 1, wobei der Sendestrahlformer (106) weiterhin variabel ist, um ein Strahlenbündel aus einer gewählten Sendeapertur auszusenden.

7. System zur diagnostischen Ultraschallbildgebung nach Anspruch 6, wobei der Sendestrahlformer (106) betriebsfähig ist, um eine Folge von Strahlenbündeln aus einer Folge unterschiedlicher Aperturen entlang des Wandlerarrays (8, 104) auszusenden.

8. System zur diagnostischen Ultraschallbildgebung nach Anspruch 7, wobei der Sendestrahlformer (106) weiterhin betriebsfähig ist, um eine Folge von Strahlenbündeln aus einer Folge unterschiedlicher Aperturen auszusenden, die so ausgewählt wurden, dass mindestens einige der lateral beabstandeten Linienpositionen von einem Strahlenbündel mit mindestens einigen der lateral beabstandeten Linienpositionen von einem anderen Strahlenbündel ausgerichtet sind.

9. System zur diagnostischen Ultraschallbildgebung nach Anspruch 8, wobei der Sendestrahlformer (106) weiterhin derartig betriebsfähig ist, dass mindestens einige der lateral beabstandeten Linienpositionen von einem Strahlenbündel mit mindestens einigen der lateral beabstandeten Linienpositionen von einem anderen Strahlenbündel koaxial ausgerichtet sind.

10. System zur diagnostischen Ultraschallbildgebung nach Anspruch 1, wobei der Mehrlinien-Empfangsstrahlformer (110a-110n) eine Vielzahl von Mehrlinien-Prozessoren umfasst, von denen jeder einen Satz von Verzögerungen auf von einer Vielzahl von Wanderelementen empfangenen Signalen anwendet, um eine Empfangs-Mehrlinie in eine ausgewählte Linienrichtung zu fokussieren.

11. System zur diagnostischen Ultraschallbildgebung nach Anspruch 10, wobei der Mehrlinien-Empfangsstrahlformer (110a-110n) eine variable Mehrlinien-Reihenfolge aufweist.

12. System zur diagnostischen Ultraschallbildgebung nach Anspruch 1, weiterhin umfassend einen mit dem Mehrlinien-Empfangsstrahlformer (110a-110n) gekoppelten Linienspeicher und betriebsfähig, um in Reaktion auf eine Vielzahl von Sendestraahlenbündeln erzeugte Empfangslinien zu speichern.

13. Verfahren zum Erzeugen eines Ultraschallbilds mit einem erweiterten Fokusbereich, wobei das Verfahren Folgendes umfasst:

Senden einer Vielzahl von Sendestraahlenbündeln (10, 20, 30) von einem Array-Wandler (8, 104) aus, wobei jedes Sendestraahlenbündel an einer anderen Position entlang des Arrays (8, 104) zentriert ist und jedes Sendestraahlenbündel (10, 20, 30) eine Vielzahl von lateral beabstandeten Linienpositionen umfasst, die in einer räumlichen Beziehung zu lateral beabstandeten Linienpositionen eines anderen Strahlenbündels stehen;

Empfangen von Echosignalen mit dem Array-Wandler (8, 104);
gleichzeitiges Verarbeiten der in Reaktion auf ein Sendestraahlenbündel (10, 20, 30) empfangenen Echosignale, um eine Vielzahl von Empfangslinien von Echosignalen an den lateral beabstandeten Linienpositionen des Strahlenbündels zu erzeugen;

Wiederholen des gleichzeitigen Verarbeitens für zusätzliche Sendestraahlenbündel (10, 20, 30);

Kombinieren von Echosignalen von Empfangslinien aus verschiedenen Sendestraahlenbündeln (10, 20, 30), die sich auf eine gemeinsame Linienposition beziehen, um Bilddaten zu erzeugen; und

Erzeugen eines Bilds unter Verwendung der Bilddaten;

gekennzeichnet durch den Schritt des Ausgleichens der Phasenverschiebungsvarianz unter allen Empfangslinien bei einer gemeinsamen Empfangslinienposition, die sich aus Sendestraahlenbündeln von unterschiedlichen Sendestraahlenorten aus ergibt, **durch** Anwenden von Verzögerungen, die sich auf den Ort jeder Empfangslinie an der gemeinsamen Empfangslinienposition relativ zu der Mitte ihres Sendestraahlenbündels beziehen.

14. Verfahren nach Anspruch 13, weiterhin umfassend das relative Gewichten der Signale von Empfangslinien aus verschiedenen Sendestraahlenbündeln vor dem Kombinieren.

Revendications

1. Système d'imagerie diagnostique par ultrasons comprenant :

une sonde (102) comportant un réseau d'éléments transducteurs (8, 104) ;

un formeur de faisceaux d'émission (106), couplé au réseau d'éléments transducteurs (8, 104), et opérationnel pour émettre un faisceau (10, 20, 30) depuis une pluralité d'emplacements de faisceau d'émission, chaque faisceau présentant une région focale et englobant une pluralité de positions de ligne espacées latéralement ;

un formeur de faisceaux de réception multiligne (110a à 110n), couplé au réseau d'éléments transducteurs (8, 104), qui est opérationnel pour produire une pluralité de lignes de réception aux positions de ligne en réponse à un faisceau d'émission (10, 20, 30) à chacun des emplacements de faisceau différents ;

un circuit combineur multiligne (114a à 114n ; 116a à 116n ; 118a à 118n ; 120), réactif à une pluralité de lignes de réception liées à une position de ligne commune produite par le formeur de faisceaux de réception multiligne (110a à 110n) en réponse à une pluralité de faisceaux d'émission (10, 20, 30), ledit circuit combineur multiligne étant opérationnel pour combiner la pluralité de lignes de réception à la position de ligne commune pour produire des données d'image ; et

un afficheur (124) qui produit une image en utilisant les données d'image ; **caractérisé en ce que**

le circuit combineur multiligne (114a à 114n ; 116a à 116n ; 118a à 118n ; 120) comporte une pluralité de retards, dans lequel un retard pour chaque ligne de réception est lié à la position de la ligne de réception à la position de ligne respective par rapport au centre de son faisceau d'émission afin d'égaliser la variance de déphasage parmi les lignes de réception de faisceaux d'émission différents à la position de ligne respective.

2. Système d'imagerie diagnostique par ultrasons selon la revendication 1, dans lequel le circuit combinateur multiligne comporte un sommateur (120) qui est opérationnel pour combiner des données de multilignes différentes.
- 5 3. Système d'imagerie diagnostique par ultrasons selon la revendication 2, dans lequel le circuit combinateur multiligne comporte en outre une pluralité de circuits de pondération (114a à 114n) qui sont opérationnels pour pondérer des données multilignes.
- 10 4. Système d'imagerie diagnostique par ultrasons selon la revendication 1, dans lequel la sonde (102) comprend une sonde à réseau linéaire.
- 5 15 5. Système d'imagerie diagnostique par ultrasons selon la revendication 1, dans lequel la sonde (102) comprend une sonde à réseau phasé.
- 15 6. Système d'imagerie diagnostique par ultrasons selon la revendication 1, dans lequel le formeur de faisceaux d'émission (106) est en outre variable pour transmettre un faisceau depuis une ouverture d'émission sélectionnée.
- 20 7. Système d'imagerie diagnostique par ultrasons selon la revendication 6, dans lequel le formeur de faisceaux d'émission (106) est opérationnel pour émettre une séquence de faisceaux depuis une séquence d'ouvertures différentes le long du réseau transducteur (8, 104).
- 25 8. Système d'imagerie diagnostique par ultrasons selon la revendication 7, dans lequel le formeur de faisceaux d'émission (106) est en outre opérationnel pour émettre une séquence de faisceaux depuis une séquence d'ouvertures différentes sélectionnée de sorte qu'au moins certaines des positions de ligne espacées latéralement d'un faisceau soient alignées avec au moins certaines des positions de ligne espacées latéralement d'un autre faisceau.
- 30 9. Système d'imagerie diagnostique par ultrasons selon la revendication 8, dans lequel le formeur de faisceaux d'émission (106) est en outre opérationnel de sorte qu'au moins certaines des positions de ligne espacées latéralement d'un faisceau soient alignées coaxialement avec au moins certaines des positions de ligne espacées latéralement d'un autre faisceau.
- 35 10. Système d'imagerie diagnostique par ultrasons selon la revendication 1, dans lequel le formeur de faisceaux de réception multiligne (110a à 110n) comporte une pluralité de processeurs multilignes, dont chacun applique un jeu de retards à des signaux reçus en provenance d'une pluralité d'éléments transducteurs pour focaliser une multiligne de réception dans une direction de ligne sélectionnée.
- 40 11. Système d'imagerie diagnostique par ultrasons selon la revendication 10, dans lequel le formeur de faisceaux de réception multiligne (110a à 110n) présente un ordre de multiligne variable.
12. Système d'imagerie diagnostique par ultrasons selon la revendication 1, comportant en outre une mémoire à lignes couplée au formeur de faisceaux de réception multiligne (110a à 110n) et opérationnelle pour mémoriser des lignes de réception produites en réponse à une pluralité de faisceaux d'émission.
13. Procédé de production d'une image par ultrasons avec une plage focale étendue, comprenant :

45 l'émission d'une pluralité de faisceaux d'émission (10, 20, 30) depuis un transducteur réseau (8, 104), chaque faisceau d'émission étant centré à une position différente le long du réseau (8, 104) et chaque faisceau d'émission (10, 20, 30) englobant une pluralité de positions de ligne espacées latéralement qui sont liées spatialement à des positions de ligne espacées latéralement d'un autre faisceau ;

50 la réception de signaux d'écho avec le transducteur réseau (8, 104) ;

le traitement simultané des signaux d'écho reçus en réponse à un faisceau d'émission (10, 20, 30) pour produire une pluralité de lignes de réception de signaux d'écho des positions de ligne espacées latéralement du faisceau ;

la répétition du traitement simultané pour des faisceaux d'émission (10, 20, 30) supplémentaires ;

la combinaison de signaux d'écho de lignes de réception provenant de faisceaux d'émission (10, 20, 30) différents liés à une position de ligne commune pour produire des données d'image ; et

55 la production d'une image en utilisant les données d'image ;

caractérisé en ce que l'étape d'égénéralisation de la variance de déphasage parmi toutes les lignes de réception à une position de ligne de réception commune résulte de faisceaux d'émission d'emplacements de faisceau d'émission différents en appliquant des retards qui sont liés à l'emplacement de chaque ligne de réception à

la position de ligne de réception commune par rapport au centre de son faisceau d'émission.

- 14.** Procédé selon la revendication 13, comprenant en outre la pondération relative des signaux de lignes de réception provenant de faisceaux d'émission différents avant combinaison.

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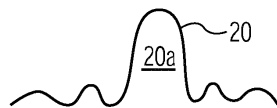
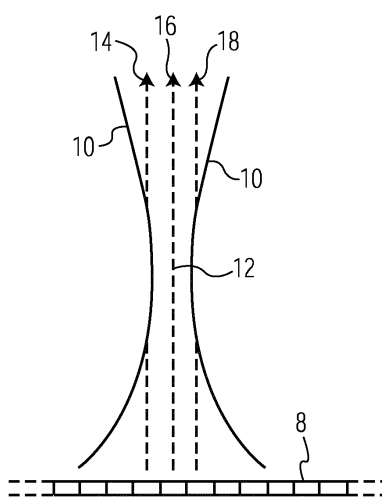


FIG. 1A

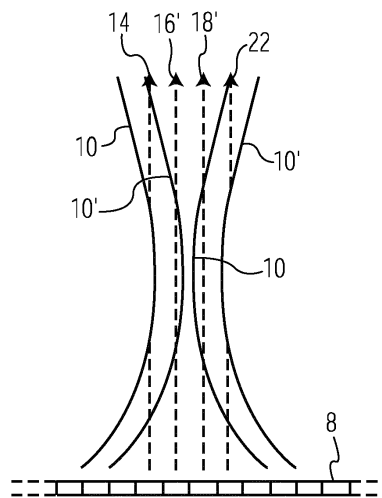


FIG. 1B

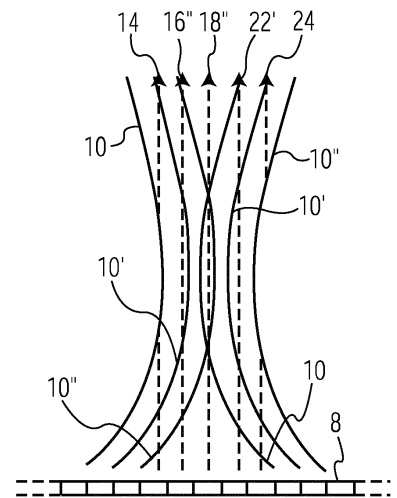


FIG. 1C

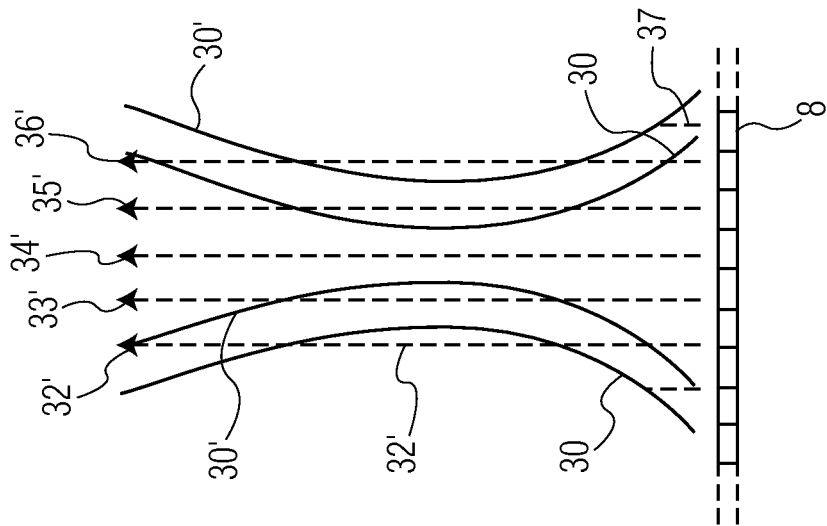


FIG. 2B

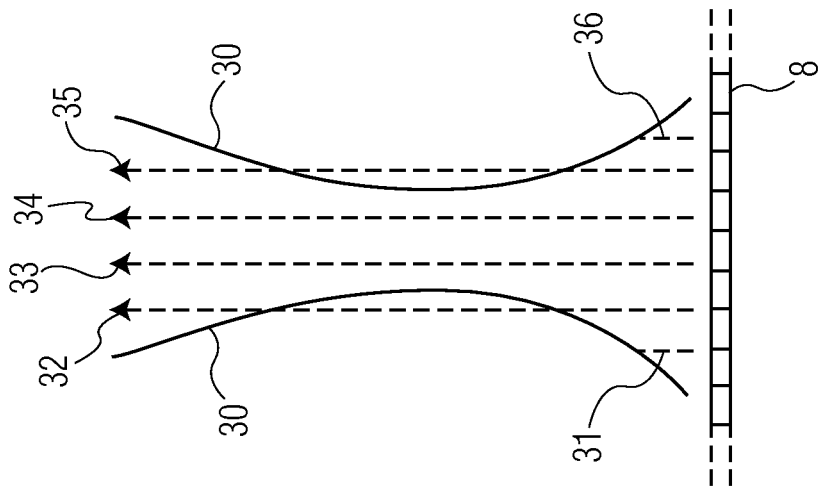


FIG. 2A

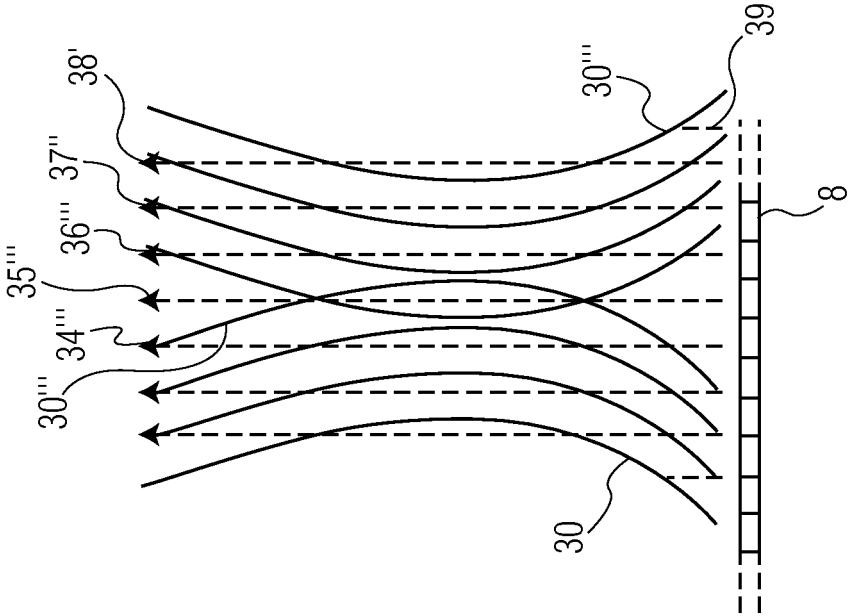


FIG. 2D

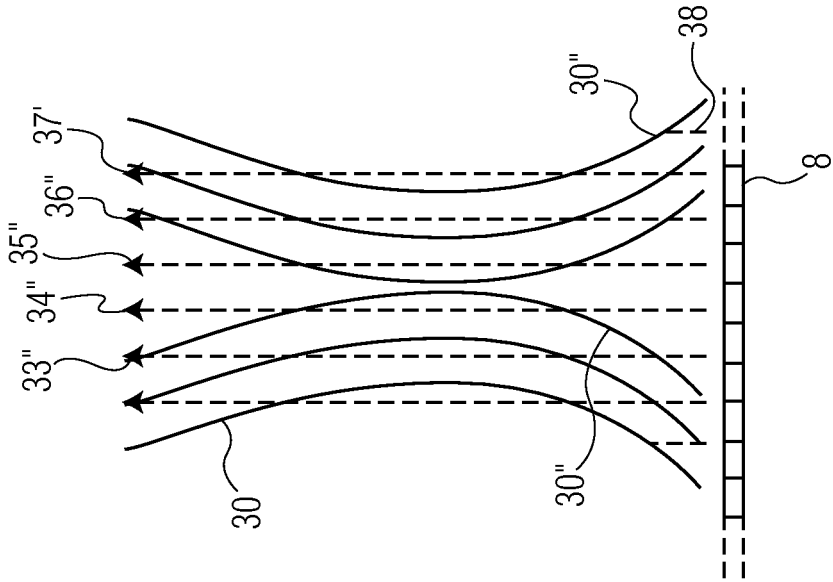


FIG. 2C

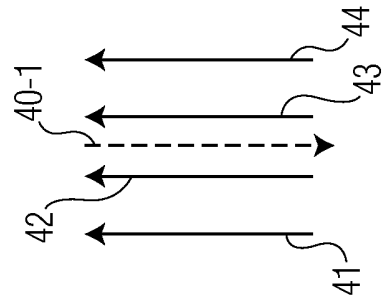


FIG. 3A

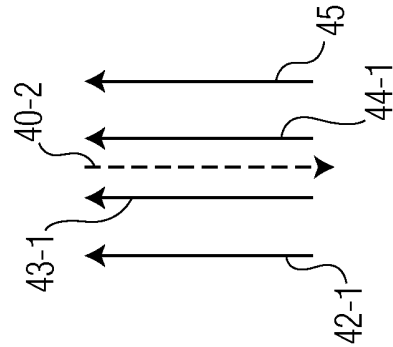


FIG. 3B

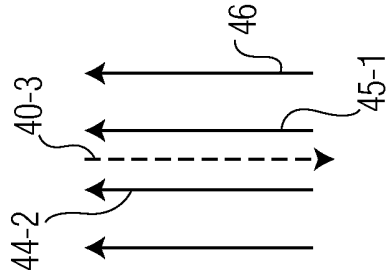


FIG. 3C

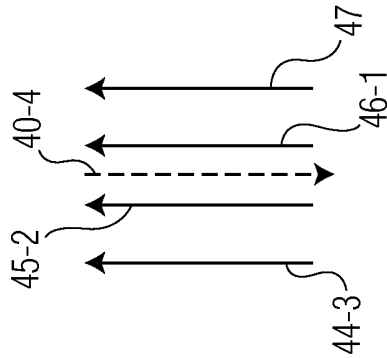


FIG. 3D

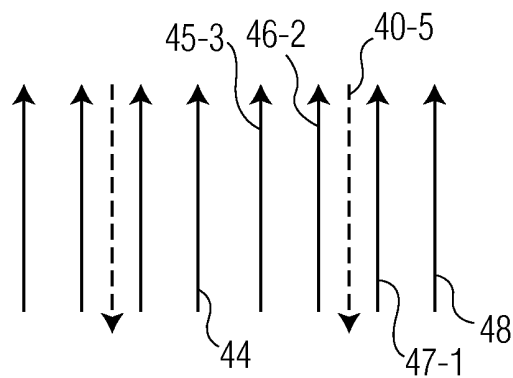


FIG. 4A

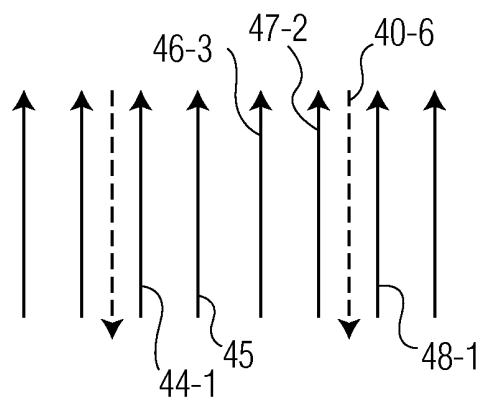


FIG. 4B

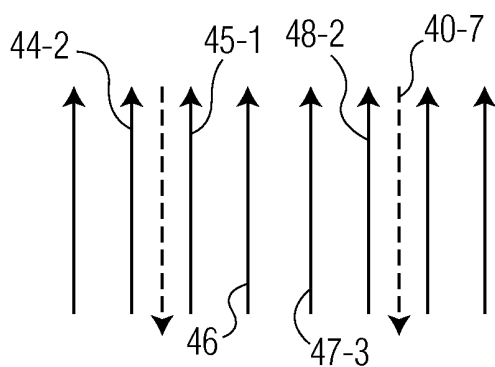


FIG. 4C

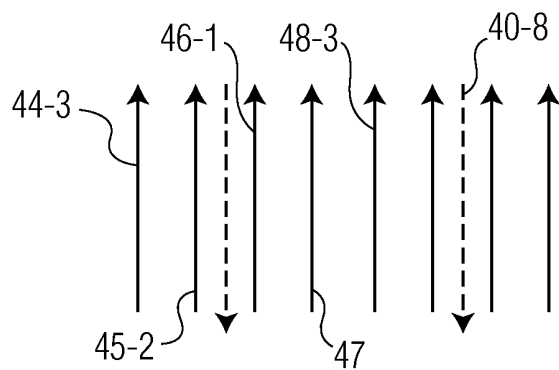


FIG. 4D

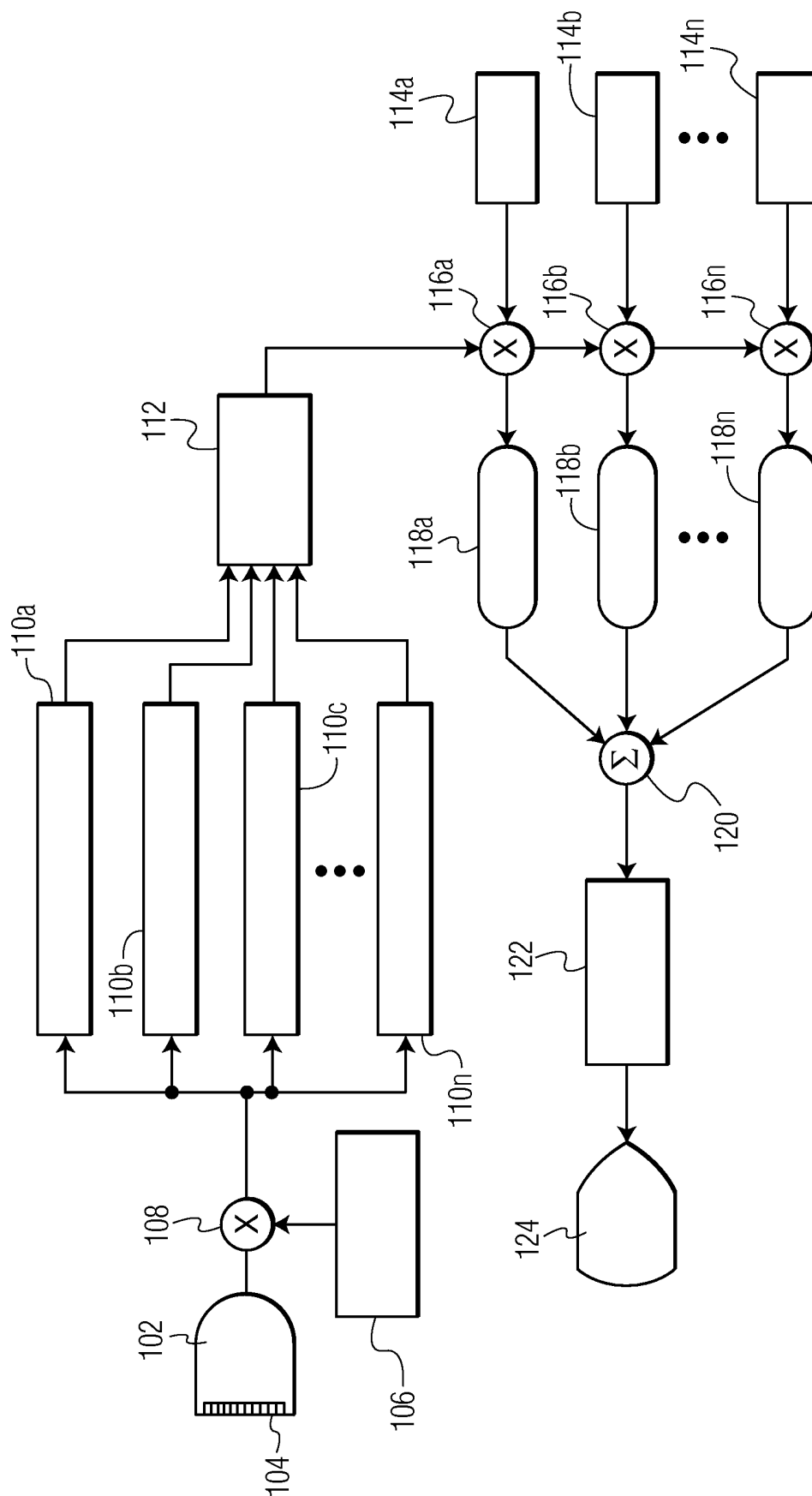


FIG. 5

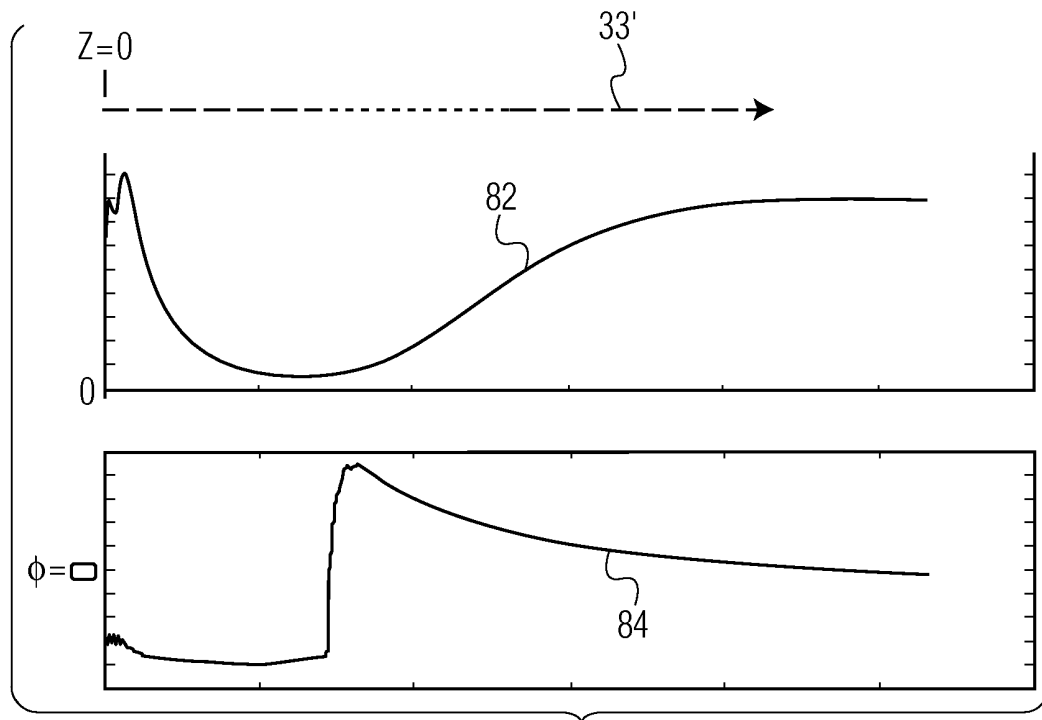


FIG. 6A

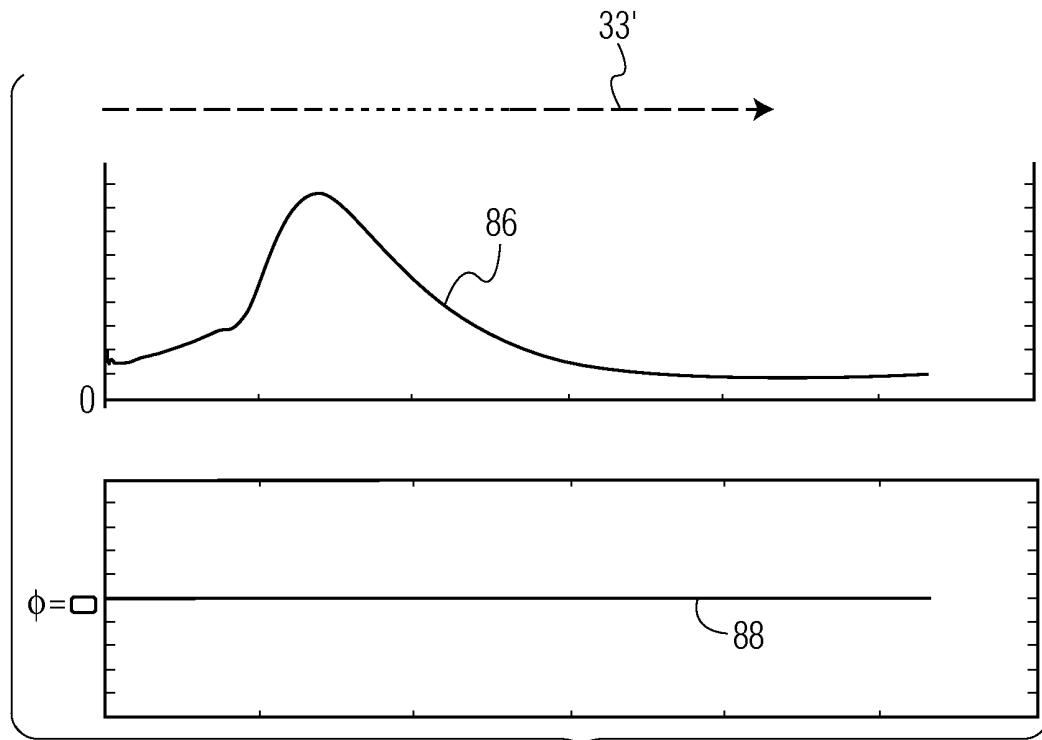


FIG. 6B

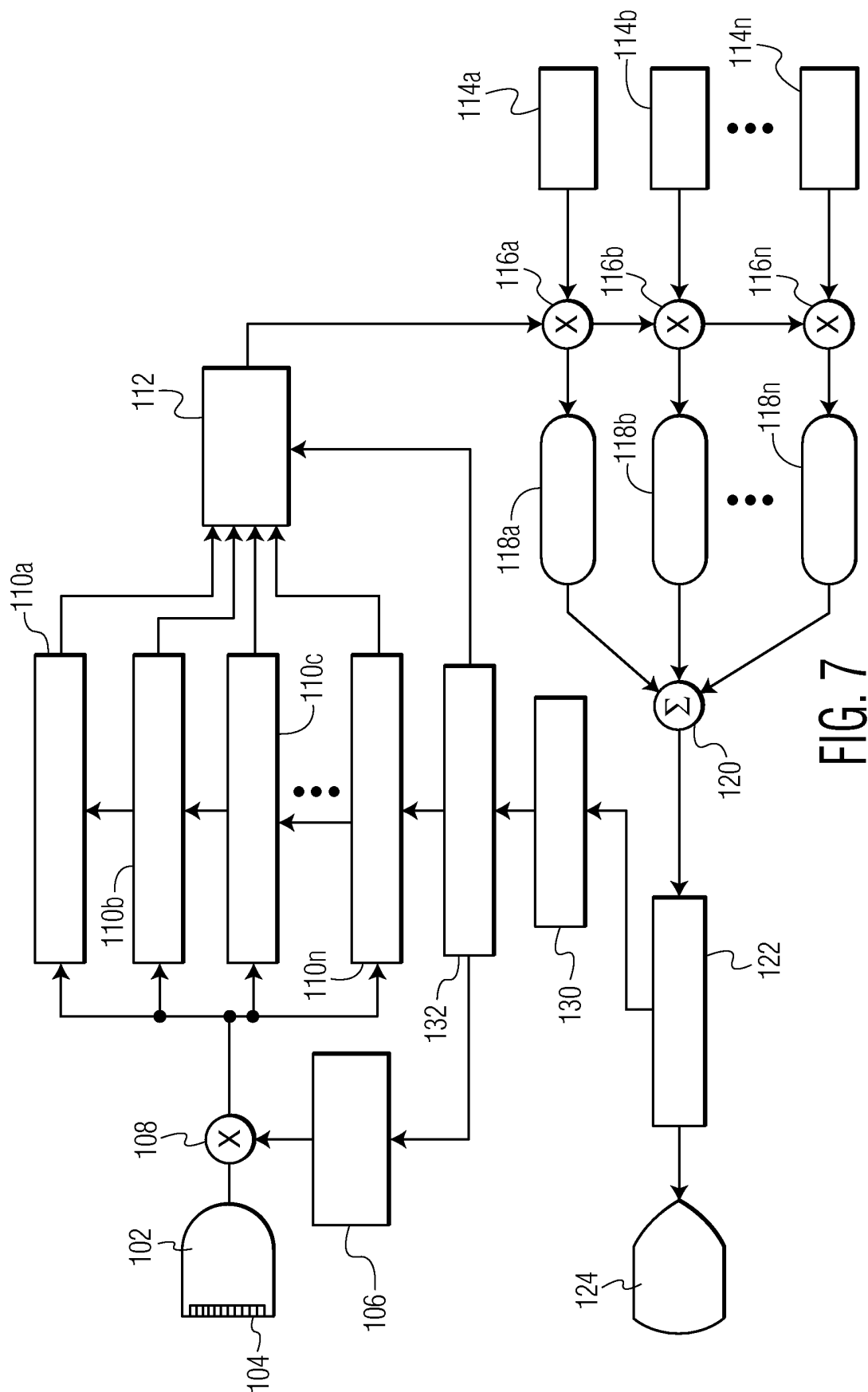


FIG. 7

REFERENCES CITED IN THE DESCRIPTION

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Patent documents cited in the description

- US 4604697 A, Luthra [0002]
- US 6231511 B, Bae [0004]
- US 5793701 A [0005]
- US 6695783 B, Henderson [0019] [0023]
- US 5318033 A, Savord [0019]
- US 6126598 A, Entrekin [0030]
- US 5127409 A, Daigle [0030]

Non-patent literature cited in the description

- **BAE et al.** A Study of Synthetic-Aperture Imaging with Virtual Source Elements in B-Mode Ultrasound Imaging Systems. *IEEE Trans. UFFC*, 2000, vol. 47 (6 [0004])

专利名称(译)	超声波合成发射聚焦与多线波束形成器		
公开(公告)号	EP2019624B1	公开(公告)日	2016-03-30
申请号	EP2007760748	申请日	2007-04-17
[标]申请(专利权)人(译)	皇家飞利浦电子股份有限公司		
申请(专利权)人(译)	皇家飞利浦电子N.V.		
当前申请(专利权)人(译)	皇家飞利浦N.V.		
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代理机构(译)	德哈恩波尔ERIK		
优先权	60/747148 2006-05-12 US		
其他公开文献	EP2019624A4 EP2019624A2		
外部链接	Espacenet		

摘要(译)

超声诊断成像系统通过发射沿阵列间隔开的多个光束来产生具有扩展焦距的图像，用于多线接收。多个发射波束的接收多线在空间上对准，并与各个接收多线之间的相位调整相结合，以防止不希望的相位消除。组合的多线产生扩展的发射焦点的效果，使得使用组合的多线产生的图像呈现扩展的焦距范围。为了防止运动伪影，多线顺序可根据图像运动进行调整。

$$\text{Weight}(x, z) = \text{amplitude}(x, z)$$