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(54) ULTRASONOGRAPH AND ULTRASONIC IMAGE DISPLAY METHOD

(57) An ultrasonic diagnostic apparatus preferable for creating a sharper image from the signal originating from contrast medium and the signal originating from biological tissues and an ultrasonic image display method are provided.

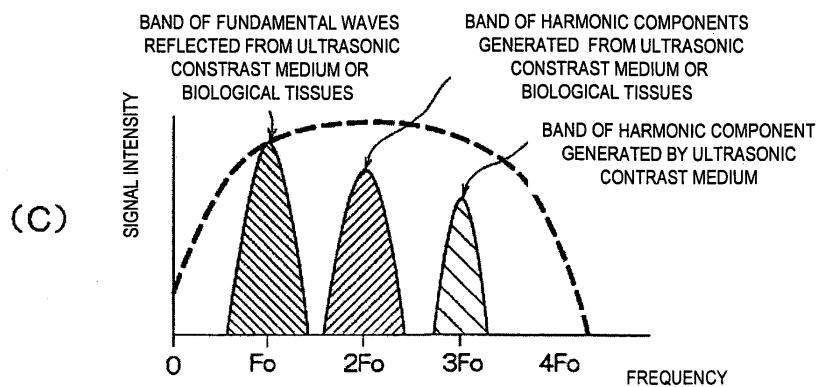
The ultrasonic diagnostic apparatus comprises an ultrasonic probe 10 for transmitting/receiving ultrasonic waves to/from an object to be examined, transmission means 12 for providing drive signals to ultrasonic probe 10, reception means for receiving the received signals outputted from ultrasonic probe 10, signal processing means 16 for processing the received signals outputted from the receiving means 14, image processing means 18 for constructing an ultrasonic image from the signals outputted from signal processing means 16, and display means for displaying the ultrasonic image.

Signal processing means 16 has means for detecting the signal intensity and the amount of variation with time of the received signal outputted from reception means 14 for each frequency band.

Image processing means 18 has means for distinguishing the signal of the ultrasonic image originating from the contrast medium and the signal originating from the biological tissues.

The signal intensity and the amount of variation with time of the received signal obtained by transmitting/receiving ultrasonic waves to/from the object are detected for each frequency band, the signals originating from the contrast medium and the biological tissues are distinguished on the basis of the signal intensity and the quantity of variation of time for each frequency band, and an ultrasonic image is displayed.

FIG. 7



Description

Technical Field

5 [0001] The present invention relates to an apparatus for imaging ultrasonic images as diagnostic images of an object to be examined and a display method thereof.

Background Art

10 [0002] An ultrasonic diagnostic apparatus for imaging ultrasonic images for diagnosis of an object to be examined is for transmitting/receiving ultrasonic waves between the object via an ultrasonic probe, and for reconstructing ultrasonic images based on the receiving signals outputted from the ultrasonic probe.

[0003] As for such ultrasonic diagnostic apparatus, a so-called harmonic imaging method is known for imaging contrast effect of ultrasonic contrast medium (hereinafter referred to as contrast medium). For example, contrast medium is 15 injected into an object and dispersed in the diagnostic region. When ultrasonic waves are irradiated to the dispersed contrast medium, harmonic components originating from nonlinearity of the medium contrast are generated. By detecting and imaging the generated harmonic components, diagnosis of blood vessel shape or discrimination of tissues is performed (for example, refer to Patent Document 1).

Patent Document 1: JP-A-H11-76231

20 [0004] Meanwhile, when ultrasonic waves are irradiated to the object to which contrast medium is injected, harmonic components not only originating from contrast medium but also originating from biological tissues of a part such as an organ are dispersed. When those harmonic components are detected and imaged, harmonic components originating from biological tissues are displayed being superimposed on the harmonic components originating from contrast medium as blind noise. Therefore, there are occasions that the contrast condition of the contrast medium cannot be grasped due 25 to difficulty in, for example, accurate visual recognition of signals originating from the contrast medium on an ultrasonic image. The method in Patent Document 1 does not address such a problem. Moreover, since a local filter is used for eliminating second harmonic components, necessary contrast echo signals are also eliminated, whereby lowering signal intensity of the contrast echo signals and deteriorating image quality.

30 [0005] Given this factor, there is a need for creating sharper images of the signals originating from contrast medium and the signals originating from biological tissues. The objective of the present invention is to provide an ultrasonic diagnostic apparatus and ultrasonic image display method capable of creating sharper images from the signals originating from contrast medium and the signals originating from biological tissues.

Disclosure of the Invention

35 [0006] In order to achieve the above-mentioned objective, the ultrasonic diagnostic apparatus of the present invention comprises:

40 an ultrasonic probe for transmitting/receiving ultrasonic waves to/from an object to be examined;
transmission means for providing drive signals to the ultrasonic probe;
reception means for receiving and processing the received signals outputted from the ultrasonic probe;
signal processing means for processing the received signals outputted from the reception means;
image processing means for constructing an ultrasonic image based on the outputted signals from the signal processing means; and
45 display means for displaying the ultrasonic image,

wherein:

50 the signal processing means comprises means for detecting signal intensity and temporal variation quantity of the received signals outputted from the receiving means for each frequency band; and
the image processing means has means for discriminating between the signals originating from contrast medium and the signals originating from biological tissues of the ultrasonic image based on the signal intensity and time variation quantity,

55 [0007] Also, the ultrasonic diagnostic apparatus of the present invention detects signal intensity and temporal variation quantity of the received signals obtained by transmitting/receiving ultrasonic waves between the objective for each frequency band, discriminates between the signals originating from contrast medium and the signals originating from the biological tissues of an ultrasonic image based on the signal intensity and time variation quantity for each frequency

band, and displays the ultrasonic image.

Brief Description of the Diagrams

5 [0008] Fig. 1 is a block diagram showing the configuration of the ultrasonic diagnostic apparatus of the first embodiment to which the present invention is applied.

Fig. 2 shows the operation of the frequency band separating means in Fig. 1.

Fig. 3 is a first diagram illustrating the operation of multiplication means in Fig. 1.

10 Fig. 4 is a second diagram illustrating the operation of multiplication means in Fig. 1.

Fig. 5 shows dyeing condition of the contrast medium with respect to the elapsed time after injection of the contrast medium.

Fig. 6 shows a display range after injection of the contrast medium.

Fig. 7 illustrates frequency characteristics of the probe in Fig. 1.

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Best Mode to Carry Out the Invention

20 [0009] An embodiment of the ultrasonic diagnostic apparatus to which the present invention is applied will be described referring to the diagrams. Fig. 1 is a block diagram showing the configuration of the ultrasonic diagnostic apparatus relating to the present embodiment.

As shown in Fig. 1, the ultrasonic diagnostic apparatus comprises:

25 wide band probe 10 (hereinafter referred to as probe 10) for transmitting/receiving ultrasonic waves to/from an object to be examined;

transmission means 12 for providing drive signals to probe 10 via transmission/reception separating means 11;

30 reception means 14 for receiving and processing the received signals outputted from probe 10 via transmission/reception separating means 11;

signal processing means 16 for processing the signals outputted from reception means 14;

image processing means 18 for reconstructing an ultrasonic image based on the received signals outputted from signal processing means 16;

35 display means 20 for displaying the ultrasonic image outputted from image processing means 18; and

control means 21 for outputting the control commands to the respective units. For the convenience of diagrammatic representation, lines indicating flow of the control commands outputted from control means 21 are omitted.

40 [0010] Here, signal processing means 16 for applying to the ultrasonic diagnostic apparatus of the present embodiment is provided with:

a plurality of signal intensity detecting means 36-1 ~ 36-m for detecting signal intensity of the received signals for each frequency band; and

45 temporal-change detecting means 22-1 ~ 22-m for detecting time variation quantity based on the signal intensity and the received signals outputted from signal intensity detecting means 36-1 ~ 36-m. Also, image processing means 18 comprises calculating means 24 for enhancement, for enhancing the signals originating from the contrast medium and the signals originating from the biological tissues of the ultrasonic image based on the signal intensity outputted from signal intensity detecting means 36-1 ~ 36-m and the time variation quantity outputted from temporal-change detecting means 22-1 ~ 22-m.

50 [0011] The ultrasonic diagnostic apparatus will now be described in more details. Probe 10 is arranged with a plurality of transducers for transmitting/receiving ultrasonic waves to/from the object. As for the transducers, transducers are applied, for example, wherein a plurality of cMUT (Capacitive Micromachined Ultrasonic Transducer: IEEE Trans, Ultrason. Ferroelectr. Freq. Contro. Vol. 45 pp. 678-690 May 1998) capable of controlling transceiver/receiver sensitivity are arranged. The transducers may have the composite piezoelectric structure in which a plurality of piezoelectric substances are arranged, or the multilayered structure in which piezoelectric substances having different resonance frequencies are laminated. The point is that it is desirable to apply the piezoelectric substances having, for example, more than 100% of fractional bandwidth for probe 10 of the present embodiment. Fractional bandwidth (FBW) here is represented as $FBW = BW/Fc$ when the center frequency is set as Fc and the bandwidth is set as BW .

55 [0012] Reception means 14 is provided with:

amplifier 26 for amplifying the received signals outputted from probe 10 via transmission/reception separating means

11;

analogue digital converter 28 (hereinafter referred to as ADC 28) for converting the received signals outputted from amplifier 26 into digital signals; and
 5 phasing addition means 30 for executing acoustic beam focusing by performing phasing addition process with respect to the received signals outputted from ADC 28.

[0013] Signal processing means 16 comprises:

10 a plurality of frequency band separating means 32-1 ~ 32-m for extracting the received signals outputted from reception means 14 by dividing them by each frequency band;

a plurality of multiplication means 34-1 ~ 34-m for multiplying predetermined coefficient to the signals outputted from the respective frequency band separating means 32-1 ~ 32-m and perform correction in accordance with propagation time of ultrasonic waves;

15 a plurality of multiplication means 34-1 ~ 34-m for multiplying the predetermined coefficient to the signal outputted from the respective frequency band separating means 32-1 ~ 32-m and correcting the multiplied signal in accordance with the ultrasonic-waves propagation time;

a plurality of signal intensity detecting means 36-1 ~ 36-m for detecting the signal intensity outputted from the respective multiplication means 34-1 ~ 34-m; and

20 a plurality of temporal change detection means 22-1 ~ 22-m for detecting time variation quantity of the signals outputted from the respective multiplication means 34-1 ~ 34-m and signal intensity detecting means 36-1 ~ 36-m. It also is provided with:

25 band control coefficient setting means 38 for setting control coefficient for the extracted band imparting to the respective frequency band separating means 32-1 ~ 32-m; and

multiplier coefficient setting means 40 for setting multiplier coefficient for imparting to the respective multiplication means 34-1 ~ 34-m. In addition, counting number m is for corresponding to the numbers of the frequency band to be extracted.

[0014] Each of frequency band separating means 32-1 ~ 32-m has a band passing filter (BPF). Signal intensity detecting means 36-1 ~ 36-m is provided with means such as absolute-value calculating means or carrier-waves eliminating means. Temporal change detecting means 22-1 ~ 22-m have a high-pass filter or quantity survey means. As for the connection mode, for example, frequency band separating means 32-1 is connected to both signal intensity detecting means 36-1 and temporal variation detecting means 22-1 via multiplication means 34-1. While frequency band separating means 32-1 was used as a representative for explaining the connection mode, other frequency band separating means 32-2 ~ 32-m are also connected to signal intensity detecting means 36-2 ~ 36-m and temporal change detecting means 22-2 ~ 22-m via multiplication means 34-2 ~ 34-m in the same manner.

[0015] Temporal change detecting means 22-1 detects temporal change parameters based on the received signals outputted from multiplication means 34-1 and the signal intensity inputted from signal intensity detecting means 36-1. Temporal parameters here indicate the unit time variation at ultrasonic wave repetition intervals, predetermined time variation summation quantity at ultrasonic wave repetition intervals, and predetermined time variation summation quantity at frame intervals. The ultrasonic wave repetition interval here corresponds to a cycle for repeatedly transmitting ultrasonic pulses from probe 10 with respect to the same scanning line (PRF), and may be referred to as a scanning repetition interval. The frame interval corresponds to the interval from the start of the transmission of ultrasonic pulses corresponding to the portion of one frame of the ultrasonic image to the start of the transmission of ultrasonic pulses corresponding to the next frame. While temporal change detecting means 22-1 was described as a representative, other temporal change detecting means 22-2 ~ 22-m operate in the same manner.

[0016] Image processing means 18 comprises a plurality of buffer memories 42-1 ~ 42-m for storing the signal intensity detected by signal intensity detecting means 36-1 ~ 36-m and the temporal change parameter detected from temporal change detecting means 22-1 ~ 22-m for each frequency band. Also, it is provided with:

50 calculation means 24 for enhancement as determination means for discriminating whether information of the respective pixels of the ultrasonic image is originating from the biological tissues or from the contrast medium, based on the signal intensity or temporal change parameter read out from the respective buffer memories 42-1 ~ 42-m;

55 color encoding table 44 for allocating color saturation, brightness and hue to the information of the respective pixels of the ultrasonic image based on the determination result of calculation means 24 for enhancement; and

frame synthesis means 46 for constructing an ultrasonic image by synthesizing the signals outputted from color encoding table 44. It also comprises table-setting means 48 for switching color maps of color encoding table 44 or adjusting hues of color maps.

[0017] Buffer memory 42-1 here sends the signal intensity or temporal change parameter to calculation means 24 for enhancement in accordance with the control commands. For example, in accordance with the desired condition such as ultrasonic measurement condition such as scan convert or zoom, diagnosis content, image reconstruction after pausing, signal intensity information and temporal change parameters are outputted to calculation means 24 for enhancement from buffer memory 42-1 in real time or resting state for the portion of continuous frames or a number of frames at several-hundred-frame intervals. While buffer memory 42-1 was described as a representative, other buffer memories 42-2 ~ 42-m operate in the same manner. As for the number of setting buffer memories 42-1 ~ 42-m, while an example for setting only the number corresponding to the number of the frequency band for separating the received signals is illustrated, it may be arbitrarily increased.

[0018] Calculation means 24 for enhancement comprises a processor having means such as four arithmetic operation means or comparison means. This processor is provided with:

a function, with respect to the three kinds of information of signal intensity, unit time variation and predetermined time variation summation which are the temporal variation parameters outputted from buffer memory 42-1, to perform quantity survey calculation in order to highlight or not to highlight the information on ultrasonic contrast medium or biological tissues and calculation for obtaining the ratio between signal intensity originating from the ultrasonic contrast medium and signal intensity originating from the biological tissues in accordance with the diagnosis content; and
 a function to allocate color display parameters such as color saturation, brightness and hue with respect to color encoding table 44 of the latter step.

[0019] Control means 21 outputs control commands to transmission means 12, reception means 14, signal processing means 16 and image processing means 18 in accordance with, for example, a command to start imaging which is outputted from input means 52. Input means 52 is configured with devices such as keyboard, mouse, switch and knob. For example, a knob is used for switching color maps or hue adjustment of table setting means 48. A switch is used for switching the kind of diagnosis.

[0020] The operation of such configured ultrasonic diagnostic apparatus will be described referring to Fig. 2 and Fig. 4. Fig. 2 illustrates an operation of frequency band separating means 32-1 ~ 32-m. Fig. 3 and Fig. 4 illustrate an operation of multiplication means 34-1 ~ 34-m.

[0021] First, ultrasonic contrast medium (hereinafter referred to as contrast medium) is injected into and dispersed in a diagnostic region. Then probe 10 is applied on a body surface of an object. In response to the command to start imaging, drive signals are generated by transmission means 12. When the generated drive signals are provided to probe 10 via transmission/reception separating means 11, ultrasonic waves are transmitted from probe 10 to the object. In this transmission, ultrasonic waves are transmitted from probe 10 at the lowest frequency (CFO) in a point of division (internal point) by which a bandwidth of probe 10 is approximately divided into n-numbers. One or a plurality of (for example, two) wave pulses are transmitted at ultrasonic-wave repeating intervals (PRF) with respect to the same scanning line. The wave pulses are transmitted with respect to the respective scanning lines in the same manner. The number of scanning lines are being set corresponding to the size of the imaging scope and azimuth direction resolution of the ultrasonic image.

[0022] The ultrasonic waves transmitted from probe 10 reflect as the reflected echoes in the process of being propagated in the body of the object. The reflected echo includes, other than fundamental harmonics, harmonic components originating from non-linearity of the contrast medium or harmonic components originating from the biological tissues. Such reflected echoes are received by probe 10. The received reflected echoes are outputted from probe 10 to reception means 14 as the received signals after being converted into electric signals.

[0023] The received signals inputted to reception means 14 are amplified by amplifier 26. The amplified received signals are converted into digital signals by ADC 28. The digitalized received signals are outputted from reception means 14 to signal processing means 16 after being phased and added by phasing addition means 30.

[0024] The received signals inputted to signal processing means 16 are inputted to frequency band separating means 32-1 ~ 32-m respectively, and here become the received signals being separated and extracted for each setting frequency band of m-number of kinds. For example, as shown in Fig. 2, the signal corresponding to the fundamental harmonics included in the received signals (F0) is extracted by frequency band separating means 32-1. The signal corresponding to the second harmonic component included in the received signals (the signals corresponding to 2F0) is extracted by frequency band separating means 32-2. The signal corresponding to the third harmonic component included in the received signals (the signals corresponding to 3F0) is extracted by frequency band separating means 32-3. Meantime, without being limited to this pattern, in addition to extracting the high order harmonic components, intermediate frequency (for example, Sub Harmonic, 1.5 Harmonic and 3rd Harmonic) may be extracted.

[0025] The intensity of the signals outputted from the respective frequency band separating means 32-1 ~ 32-m is corrected by multiplication means 34-1 ~ 34-m as shown in Fig. 3. For example, the received signal outputted from

frequency band separating means 32-1 is inputted to multiplication means 34-1, the predetermined multiplier coefficient is multiplied here to the signal and the signal intensity is corrected. In the same manner, the received signal outputted from frequency-band separating means 32-2 is corrected by multiplication means 34-2, and the received signal outputted from frequency band separating means 32-3 is corrected by multiplication means 34-3 respectively.

5 [0026] The multiplier coefficient here is variably controlled by multiplication means 40, for example as shown in Fig. 4, with respect to the propagation time of ultrasonic waves in every frequency band that is every multiplication means 34-1 ~ 34-m. More concretely, as for the received signals (F0), multiplier coefficient is increased in approximate proportion to the increase of propagation time of the ultrasonic waves. As for the received signal (2F0), the multiplier coefficient is gradually increased up to the predetermined propagation time of ultrasonic waves, and after passing that time the multiplier coefficient is gradually decreased. As for the received signal (3F0), the multiplier coefficient is variably changed basically in the same manner as the case of the received signal (2F0), but the propagation time of ultrasonic waves where the multiplier coefficient reaches the maximum is shorter than the case of the received signal (F20). By variably controlling the multiplier coefficient with respect to the ultrasonic waves propagation time, lowering of the signal intensity due to the attenuation or dispersion generated in the propagation process of ultrasonic waves in the body of the object can be corrected.

10 [0027] The respective received signals corrected by multiplication means 34-1 ~ 34-m are inputted to both signal intensity detecting means 36-1 ~ 36-m and temporal change detecting means 22-1 ~ 22-m. The received signals inputted to signal intensity detecting means 36-1 ~ 36-m are performed with a process such as absolute value calculation or elimination process of carrier waves. Through such process, the signal intensity can be detected for each setting frequency band of m-number of kinds. The detected signal intensity is outputted to temporal change detecting means 22-1 ~ 22-m, and maintained in buffer memories 42-1 ~ 42-m.

15 [0028] On the other hand, in temporal change detecting means 22-1 ~ 22-m, temporal change parameter is detected for each set frequency band of m-number of kinds based on the received signals inputted via multiplication means 34-1 ~ 34-m and the signal intensity inputted from signal intensity detecting means 36-1 ~ 36-m. The temporal change parameters here are a unit time variation quantity at ultrasonic waves repeating intervals, predetermined time variation summation at ultrasonic waves repeating intervals and predetermined time variation summation at frame intervals. For example, when the signal intensity is set as $I(t)$, the temporal change parameter of each frequency band can be obtained by temporal change detecting means 22-1 ~ 22-m as shown in chart 1. The obtained temporal change parameter is maintained in buffer memories 42-1 ~ 42-m for each frequency band of m-number of kinds.

30

[Chart 1]

		Temporal change parameters	
35	Unit time variation	Ultrasonic wave repetition interval frequency tp Frame interval frequency tf	$ dI(tp)/dtp $ $ dI(tf)/drf $
40	Predetermined-time variation summation	Ultrasonic wave repetition interval frequency tp Frame interval frequency tf	$\Sigma (dI(tp)/dtp)$ $\Sigma (dI(tf)/dtp)$

45 [0029] More description of the temporal change parameters will be added here. As for the unit time variation quantity, it turns out large when the signal intensity is high and the change is drastic, and it turns out small when the signal intensity is low and the change is moderate. The predetermined time variation summation is a summation of the unit time variation quantity in a predetermined time, which turns out large when the unit time variation of the predetermined time is large and continuous, and turns out small when the unit time variation is small and occurs singly. More concretely, as for the contrast medium, static biological tissues (for example, a kidney), dynamic biological tissues (for example, a heart or blood vessel) and blood cells, the ultrasonic frequency band and time variation quantity have characteristics as shown in Fig. 2. As seen in Fig. 2, the characteristics of the contrast medium are a point that the signal intensity turns out large due to a big difference in acoustic impedance compared to the biological tissues, a point that the fundamental harmonic, second harmonic and third harmonic turn out all large since the volume change by irradiation of ultrasonic waves are non-linearly oscillated, and a point that the unit time variation quantity and predetermined time variation summation turn out large since they are comparatively movable. The characteristic of the biological tissues is that the third harmonic component is comparatively small since the volume does not change compared to the contrast medium. For example, the characteristic of static biological tissues is that while signal intensity turns out large, unit time variation quantity and predetermined time variation quantity turn out small due to their small movement. The characteristic of dynamic biological tissues is that while signal intensity turns out large, the unit time variation quantity at ultrasonic wave repetition intervals turns out comparatively small and the predetermined time variation summation at frame intervals turns out large due to

their slow movement. The characteristic of blood cells is that while the signal intensity turns out smaller than the biological tissues, the unit time variation quantity and predetermined time variation summation quantity turn out larger than the static biological tissues due to their free movement within the body.

		[Chart 2]			
		Contrast medium	Blood cell	Static organism	Dynamic organism
10	Signal, intensity	Fundamental harmonics	Large	Intermediate	Large
		Second harmonic component	Large	Intermediate	Large
		Third harmonic component	Large	Small	Small
15	Unit time variation quantity	Ultrasonic wave repetition interval	Large	Intermediate	Small
20	Predetermined time variation summation	Ultrasonic wave repetition interval	Large	Intermediate	Small
25		Frame interval	Large	Intermediate	Large

[0030] The signal intensity or temporal variation parameters maintained in buffer memories 42-1 ~ 42-m are read out by calculation means 24 for enhancement. At this time, scan convert, zoom or measurement condition of ultrasonic waves are read out in accordance with desired condition such as image reconstruction after pausing. Based on the read out signal intensity or temporal change parameters, determination is made whether the information of the respective pixels of the ultrasonic image is originating from the biological tissues or from the contrast medium by calculation means 24 for enhancement. Then based on the determination result of calculation means 24 for enhancement, color saturation, brightness and hue are allocated to the information of the respective pixels of the ultrasonic image by color encoding table 44. Based on the signals outputted from color encoding table 44, an ultrasonic image is constructed by frame synthesis means 46. The constructed ultrasonic image is displayed on display means 20.

[0031] More details of the processing content of calculation means 24 for enhancement will now be described. First, the respective signals that are separated into the respective frequency bands by signal processing means 16 are the signals on which the signal originating from contrast medium and the signal originating from biological tissues are superimposed. Much the same is true on the signal of a fundamental harmonic "Sig(F0)", the signal of a second higher harmonic (2F0) and the signal of a third higher harmonic (3F0).

[0032] By calculation means 24 for enhancement, formula (1) is expressed as an arithmetic expression for enhancing the signal from medium contrast and the signal from biological tissues. A, B and C of formula (1) is the weighting factor to be multiplied to the respective signals.

$$A \cdot \text{Sig}(F0) + B \cdot \text{Sig}(2F0) + C \cdot \text{Sig}(3F0) \quad (1)$$

Based on formula (1), calculation by the signal enhancing coefficient originating from the medium contrast, calculation by the signal enhancing coefficient originating from the biological tissues and calculation without enhancement process are performed by calculation means 24 for enhancement. More concretely, medium contrast, in addition to nonlinear phenomenon due to propagation of ultrasonic waves in the elastic body, has resonance frequency from the result of hardness and inertia in accordance with the original radius of the contrast medium (For example, IEEE Ultrasonics Symposium 1996 P1451). Consequently, while the signal originating from the contrast medium has a certain degree of signal intensity in the higher harmonics of a comparatively high order, the signal originating from the biological tissues has small signal intensity in the higher harmonics of a comparatively high order. Therefore, when it is desired to highlight the signals originating from the contrast medium, formula (1) should be calculated by making the weighting coefficient as "C=1, A=B=0". When it is desired to highlight the signals originating from the biological tissues, formula (1) should be calculated by making the weighting coefficient as "A=0.5~1.0, B=0.5~1.0, C=0~1.0". Summation of A, B and C here is set at a steady value (for example, "1"). Also, in the case not to implement the enhancement process, formula

(1) should be calculated by making the weighting coefficient as " $C=A=B=1/3$ ".

[0033] The calculation result (summation) of formula (1) is applied for determining the signals originating from contrast medium and the signals originating from biological tissues, by using in conjunction with the temporal change parameters in calculation means 24 for enhancement. More concretely, by performing calculation for enhancing the signals originating from the biological tissues by the signal intensity coefficient originating from the biological tissues, calculation for enhancing the signals originating from the contrast medium by the signal intensity coefficient originating from contrast medium and calculation without enhancement based on formula (1) with respect to each of the three information of the signal intensity, unit time variation quantity and predetermined time variation summation of calculation means 24 for enhancement, for example, of $\text{Sig}(F0)$, a total of 9 signals are generated. Also, the signal intensity ratio of the signals originating from the biological tissues and the contrast medium are calculated. Such calculation process is executed on an image pixel basis.

[0034] Next, based on the 9 signals and the signal intensity ratio, color saturation, brightness or hue is allocated on an image pixel basis by color encoding table 44. For example, the signal that is not performed with enhancement process of the unit time variation quantity at ultrasonic wave repetition interval is used for the color saturation, and the hue of red is used for enhancing the contrast medium and blue is used for enhancing the biological tissues, by the signal intensity ratio between the signals originating from the biological tissues and the signals originating from the contrast medium with respect to the signal intensity. By such process, the image originating from the contrast medium is dyed in bright red, the image originating from the static biological tissues is dyed in light cobalt blue, and the image originating from the dynamic biological tissues is dyed in light blue. Such color mapping is also effective for the diagnosis of the blood vessel condition such as a tumor, as the real-time diagnosis of the vascular phase.

[0035] Also, the region dyed with contrast medium may be highlighted by simply allocating red to the signal originating from the contrast medium and blue to the signal originating from the biological tissues with respect to the signal intensity, and superimposing and color-displaying the respective signals. The point is that calculation means 24 for enhancement is to select the combination for allocating the 9 signals and the signal intensity ratio with respect to color encoding table 44. By displaying the ultrasonic image allocated with information such as color saturation by color encoding table 44, it is possible to facilitate discrimination between the image originating from the contrast medium and the image originating from the biological tissues.

[0036] Such ultrasonic diagnostic apparatus can be applied to discrimination of tissue characterization based on the dyeing condition of the image using contract medium. Tissue characterization here means the condition, predisposition or benignancy/malignancy of the tissues. Fig. 5 is an example of the tissue differential diagnosis, and shows the dyeing condition of the image after the injection of contrast medium with respect to the elapsed time. The horizontal axis in Fig. 5 indicates the elapsed time after the injection of contrast medium, and the vertical axis indicates the signal intensity. As shown in Fig. 5, a blood vessel is dyed with contrast medium in early phase, and the rising and falling of dyeing condition of the image are precipitous. A portal starts to be dyed in the early phase later than the starting time of the blood vessel, and the rising of dyeing condition is precipitous but the falling is moderate. A liver starts to be dyed from the intermediate phase, and both rising and falling of the dyeing condition are moderate. A tumor with many new blood vessels starts to be dyed in early phase, and the falling of dyeing condition is moderate. A tumor with necrosis does not get dyed. By such dyeing mechanism, it is possible to make an effective differential diagnosis of pathologic tissues.

[0037] Differential diagnosis of the tissue characterization based on the dyeing condition of the contrast medium will be further described referring to Fig. 5 and Chart 3. Chart 3 shows the elapsed time after the injection of contrast medium into a liver and the dyeing condition of the image using contrast medium of a blood vessel, liver cell and liver cancer. The contrast medium injected into a living body is gradually circulated from the blood vessel around the whole body, and discharged outside the body over time by lung or kidney function. The contrast medium preyed by the engulfment cells, etc. stays in the body for comparatively a long time. Here, when the elapsed time from the injection of contrast medium is sectionalized into early stage, intermediate state and late stage, for example, the contrast medium intensity in the blood vessel increases drastically from the injection start time, and moderately decreases after reaching a certain time. Therefore, the unit time variation quantity, predetermined time variation summation and signal intensity summation of the signal originating from inside of the blood vessel turn out large at the early stage. Also, in the intermediate and late stage, the unit time variation quantity, predetermined time variation summation and signal intensity summation turn out small due to lowering of the intensity of contrast medium in the blood vessel.

[0038] The contrast medium intensity of the liver cell moderately increases from the intermediate stage, and stays very long time due to the prey by the engulfment cells. Consequently, the unit time variation quantity, predetermined time variation summation and signal intensity summation of the signals originating from the liver cell turn out small at the early stage. Also, they turn out gradually larger at the intermediate stage, and reach maximum at the late stage.

[0039] Contrast medium intensity in the liver cancer drastically increases from the start time of injection at the early stage as in the same manner as the blood vessel, and drastically decreases after reaching a certain time, due to the existence of numerous new blood vessels. Consequently, the unit time variation, predetermined time variation summation and signal intensity summation of the signal originating from the liver cancer turn out large at the early stage. Also, being

different from the blood vessel, the unit time variation quantity, predetermined variation summation and signal intensity summation keep a certain value in the intermediate stage since the incorrect holes existing in the new blood vessels are prone to be clogged with the contract medium. Also, the time variation quantity, predetermined time variation summation and signal intensity summation turn out small in the late stage since there is no engulfment cell. In this way, in the liver, the elapsed time after injection of the contrast medium and the dyeing condition of the contrast medium in the blood vessel, liver cell and liver cancer are different. In addition, while an example for discrimination of the tissues in the liver is described, the tissue discrimination can also be applied to the tissues of the other organs. For example, in a circulatory system, the dyeing time is different between the blood vessel flowing directly from the heart to the biological tissues and the portal passing through the small intestine. Also, there are occasions that necrosis tissues where there is no blood flow and bouton, etc. do not get dyed. In this way, by the visual recognition of the sharp image using the contrast medium, tissue characterization of the liver cell can be accurately discriminated.

[Chart 3]

		In a blood vessel	Liver cell (engulfment cell)	Liver cancer (no neovascularity or engulfment cell)
15	Early stage	Unit time variation	Large	Small
		Predetermined time variation summation	Large	Small
		Signal intensity summation	Large	Small
20	Intermediate stage	Unit time variation	Small	Intermediate
		Predetermined time variation summation	Small	Intermediate
		Signal intensity summation	Small	Large
25	Late stage	Unit time variation	Small	Large
		Predetermined time variation summation	Small	Large
		Signal intensity summation	Small	Intermediate
30	Late stage	Unit time variation	Small	Intermediate
		Predetermined time variation summation	Small	Intermediate
		Signal intensity summation	Small	Large
35	Late stage	Unit time variation	Small	Large
		Predetermined time variation summation	Small	Large
		Signal intensity summation	Small	Intermediate

[0040] More specifically, as an example of color mapping for discriminating the tissue characterization, the coefficient is set for enhancing the contrast medium, color saturation is set for the unit time variation quantity at ultrasonic wave repetition intervals, and brightness is set for the time variation quantity at frame intervals. Then the red hue is allocated to the early phase of the elapsed time after injection of the contrast medium, green hue is allocated to the intermediate phase, and blue hue is allocated to the late phase. By doing so, the dyeing condition of the contrast medium can be determined. For example, determination can be made whether the rising and falling of the dyeing in the imaging is precipitous or not. Also, determination can be made as to whether the dyeing continues or not. Further, determination can be made as to which of the early phase, intermediate phase and late phase is being dyed with contrast medium or not dyed. On the basis of such dyeing condition, it is possible to discriminate the tissue characterization. Color mapping of the present embodiment may be applied to the case of static images, images once stored or abdominal examination using the on-the-fly processing.

[0041] In concrete terms, referring to Fig. 5, when attention is on the liver and the liver is colored in red at the early phase and is colored in green at the intermediate phase, it is possible to determine that the colored region thereof is a liver cancer. In particular, only the liver cancer is colored in the liver at the anterior half of the intermediate phase, it is possible to recognize the whereabouts of the liver cancer by merely observing the phase. In color encoding table 44, it is possible to display only the liver cancer region by setting so as to display only the colored region at the anterior half of the intermediate phase. Then the image created from the signal originating from the biological tissues and the image colored only in the liver cancer are superimposed by frame synthesis means 46. Through such creation of the ultrasonic waves, it is possible to identify in what region the liver cancer exists in the living body.

[0042] As shown in Fig. 6, bar 100 for selectively displaying the signal originating from the contrast medium is displayed on the lower part of display means 20, and the signal originating from the contrast medium is selectively displayed using

input means 52. Time phase bar 100 is divided into an early phase, intermediate phase and late phase. The borderlines between these phases are indicated by a dotted line. On time phase bar 100, starting point 101 for indicating the start and ending point 102 for indicating the end are displayed. Starting point 101 and ending point 102 are operated by input device 52, the operated information is transmitted to control unit 21, and color encoding table 44 is controlled by control unit 21. Color encoding table 44 performs coloring using the signals between starting point 101 and ending point 102 that are originating from the contrast medium.

5 [0043] The coloring starts from the phase in which starting point 101 is displayed, and it ends at the phase in which ending point 102 is displayed. In an example of Fig. 6, it is possible to display only the liver cancer region by setting starting point 101 and ending point 102 in the anterior half of the intermediate phase so as to display only the region colored in the anterior half of the intermediate phase. When it is desired to observe only the liver cells, starting point 101 and ending point 102 are to be set in the posterior half of the late phase.

10 [0044] As described above, in accordance with the present embodiment, it is possible to determine whether the information of the ultrasonic image in each pixel is originating from medium contrast or from biological tissues, by extracting the time variation quantity of the received signals outputted from reception means 14 for each frequency band 15 and detecting the intensity and time variation quantity of each signal. As a result, by enhancing and color displaying the signals originating from the contrast medium and from the biological tissues based on the determination result, each signal originating from the contrast medium and from the biological tissues can be clearly imaged.

In this way, even in the case that the discrimination of tissue characterization is performed on the basis of dyeing condition 20 of the contrast medium, a sharper dyed-image can be obtained whereby enabling accurate tissue discrimination.

25 [0045] Also, the color ultrasonic image of the present embodiment may be displayed by imaging a black and white tomographic image before injecting contrast medium into an object, and juxtapose or superimpose the imaged black and white tomographic image to or on the color ultrasonic image. By doing so, the black and white tomographic image becomes the background image with respect to the color ultrasonic image whereby making it easier to carry on the procedure while visually observing the organ for diagnosis on the image.

30 [0046] Here, probe 10 of the present embodiment will be described in detail. Since the probe having, for example, more than 100% of fractional bandwidth is used for probe 10 of the present embodiment, even higher harmonics of 35 comparatively high order can be received with high sensitivity. This point will be explained referring to Fig. 7. Fig. 7A shows the frequency band characteristics of probe 10 relating to the present embodiment by a dotted line. Fig. 7B shows the frequency band of the ultrasonic wave transmitted from probe 10. Fig. 7C shows the frequency band of the ultrasonic wave received from probe 10. The horizontal line of Fig. 7 denotes the frequency, and the vertical line denotes the signal intensity. The frequency band is denoted as lower band F0, central band 2F0 and higher band 3F0.

40 [0047] First, as comparison with the present embodiment, the case of the probe arrayed with transducers formed with PZT (piezoelectric zirconate titanate) will be described. This probe has degree of 60% ~ 80% of fractional bandwidth, thus has the frequency band in the case, for example, that the center frequency if 5MHz, from 3MHz of lower band 45 frequency to 7MHz of higher frequency. Here, if the ultrasonic-wave transmitting frequency is set as 3MHz, the second higher harmonic is 6MHz and the third higher harmonic is 9MHz. However, since the third higher harmonic 9MHz is more than 7MHz of the high-pass frequency of the probe that is out of its frequency band, there are cases that the sensitivity is drastically lowered. Also, though a method is available to receive higher harmonics within the frequency band by setting the transmission frequency at a lower frequency that is, for example, 2MHz and setting the second higher harmonic as 4MHz and the third higher harmonic as 6MHz, it can be a cause of inefficiency since the transmission frequency is out of the frequency band.

45 [0048] In this regard, since probe 10 of the present embodiment has more than 100% of fractional bandwidth, when the central frequency is, for example, 5MHz, the frequency band will be from 2.5MHz of the low-pass frequency to 7.5MHz of the high-pass frequency. Here, if transmission frequency (F0) of probe 10 is set as 2.5MHz as shown in Fig. 50 7B, the higher components can be received within the frequency band with second higher harmonic (2F0) being 5MHz and third higher harmonics (3F0) being 7.5MHz as shown in Fig. 7C. In other words, fundamental harmonics band originating from the contrast medium or from the biological tissues and the signal of the higher harmonic band originating from the contrast medium or the biological tissues can be received with high sensitivity.

In conclusion, since it is possible to receive even higher harmonics of comparatively high order, it is possible to create sharper images of the signals originating from the contrast medium or from the biological tissues.

Claims

55 1. An ultrasonic diagnostic apparatus comprising:

an ultrasonic probe for transmitting/receiving ultrasonic waves over a predetermined period of time between an object into which contrast medium is injected;

transmission means for providing drive signals to the ultrasonic probe;
 reception means for receiving and processing the received signals outputted from the ultrasonic probe;
 signal processing means for processing the received signals outputted from the reception means;
 5 image processing means for constructing an ultrasonic image based on the signals outputted from the signal processing means; and
 display means for displaying the ultrasonic image,

wherein:

10 the signal processing means has means for detecting signal intensity and time variation quantity of the received signals outputted from the reception means for each frequency band, and
 the image processing means has means for determining whether the received signal is originating from the contrast medium or from the biological tissues based on the signal intensity and the time variation quantity of the received signal.

15 2. The ultrasonic diagnostic apparatus according to claim 1, wherein the image processing means allocates a hue different from the signal originating from the biological tissues to the ultrasonic image of the signal originating from the contrast medium based on the elapsed time after an injection of the contrast medium, and displays the image on the display means.

20 3. The ultrasonic diagnostic apparatus according to claim 7, **characterized in that** the image processing means allocates the first hue to the early phase in the elapsed time after the injection of contrast medium, the second hue to the intermediate phase and the third hue to the late phase with respect to the ultrasonic image of the signals originating from the contrast medium, and displays the image on the display means.

25 4. The ultrasonic diagnostic apparatus according to claim 1, wherein the image processing means comprises calculating means for enhancement, for determining the signal originating from the contrast medium and the signal originating from the biological tissues for each pixel of the ultrasonic image for each frequency band, based on the signal intensity and time variation quantity of the received signals.

30 5. The ultrasonic diagnostic apparatus according to claim 4, wherein the image processing means has a color encoding table for allocating at least one of color saturation, brightness and hue to the information of each pixel on the ultrasonic image, based on the determination result of the calculation means for enhancement.

35 6. The ultrasonic diagnostic apparatus according to claim 4, wherein:

the calculation means for enhancement determines the dyeing condition of the contrast medium for each set phase since the time of injecting the contrast medium; and
 40 the color encoding table updates at least one of the color saturation, brightness and hue at each determination process performed by the calculation means for enhancement.

45 7. The ultrasonic diagnostic apparatus according to claim 1, wherein the image processing means comprises a plurality of buffer memories for storing the signal intensity and time variation quantity detected by the signal processing means for each frequency band.

8. The ultrasonic diagnostic apparatus according to claim 7, **characterized in** comprising determination means for determining whether the information of the respective pixels of an ultrasonic image is originating from the biological tissues or from the contrast medium, based on the signal intensity or temporal change parameters read out from the plurality of buffer memories.

50 9. The ultrasonic diagnostic apparatus according to claim 8, wherein the image processing means images a black and white tomographic image before the injection of contrast medium into the object, and juxtaposes or superimposes the black and white tomographic image on or to a color ultrasonic image.

55 10. The ultrasonic diagnostic apparatus according to claim 1, wherein the signal processing means has temporal change detecting means for detecting the temporal change parameters which are a unit time variation quantity at ultrasonic-wave repetition intervals, predetermined time variation summation at ultrasonic-wave repetition intervals and pre-determined time variation summation at frame intervals.

11. The ultrasonic diagnostic apparatus according to claim 1, wherein the signal processing means detects, as the time variation quantity, at least one of the unit time variation quantity and the time variation quantity of predetermined time which is longer than the unit time variation thereof.

5 12. The ultrasonic diagnostic apparatus according to claim 1, wherein the signal processing means detects, as the time variation quantity, at least one of the time variation quantity at ultrasonic-wave repetition intervals and the time variation quantity at frame intervals.

10 13. The ultrasonic diagnostic apparatus according to claim 1, wherein the signal processing means has:

a plurality of frequency band separating means for extracting the received signals outputted from the reception means by dividing them by frequency bands;

a plurality of multiplication means for correcting the signals outputted from the respective frequency band separating means in accordance with the ultrasonic-wave propagation time;

15 signal intensity detecting means for detecting the intensity of the signal outputted from the respective multiplication means; and

temporal change detecting means for obtaining the time variation quantity based on the signals outputted from the multiplication means and the signal intensity outputted from the signal intensity detecting means.

20 14. The ultrasonic diagnostic apparatus according to claim 13, wherein the multiplication means variably controls for each frequency band.

15 15. The ultrasonic diagnostic apparatus according to claim 13, wherein the multiplication means changes weighting function, in the case of enhancing the signals originating from the biological tissues or from the contrast medium.

25 16. The ultrasonic diagnostic apparatus according to claim 1, wherein the ultrasonic probe has comparison ratio that is larger than 100%.

30 17. The ultrasonic diagnostic apparatus according to claim 1, wherein the ultrasonic probe is configured with transducers by cMUT.

35 18. The ultrasonic diagnostic apparatus according to claim 1, comprising a plurality of frequency band separating means for extracting the received signals by dividing them by frequency bands, **characterized in that** each of them has a band pass filter.

19. The ultrasonic diagnostic apparatus according to claim 2, wherein the image processing means has selecting means for selecting the signals originating from the contrast medium to be displayed on display means in the elapsed time.

40 20. An ultrasonic image display means **characterized in:**

detecting the signal intensity and time variation quantity of the received signals obtained by transmitting/receiving ultrasonic waves between an object for each frequency band;

determining the signal originating from contrast medium and from biological tissues of an ultrasonic image based on the signal intensity and time variation quantity for each frequency band; and

45 displaying the ultrasonic image.

50

55

FIG.

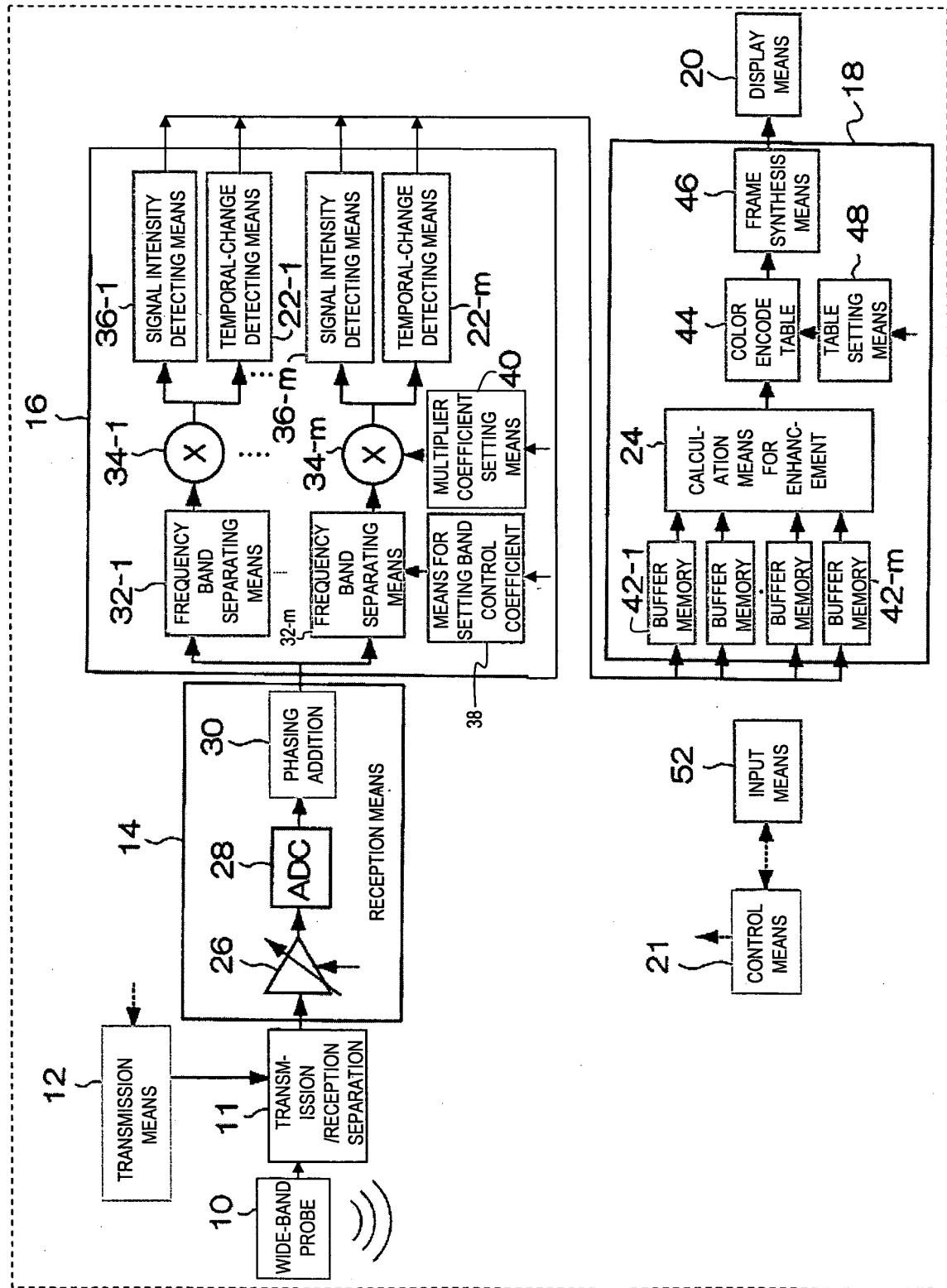


FIG.2

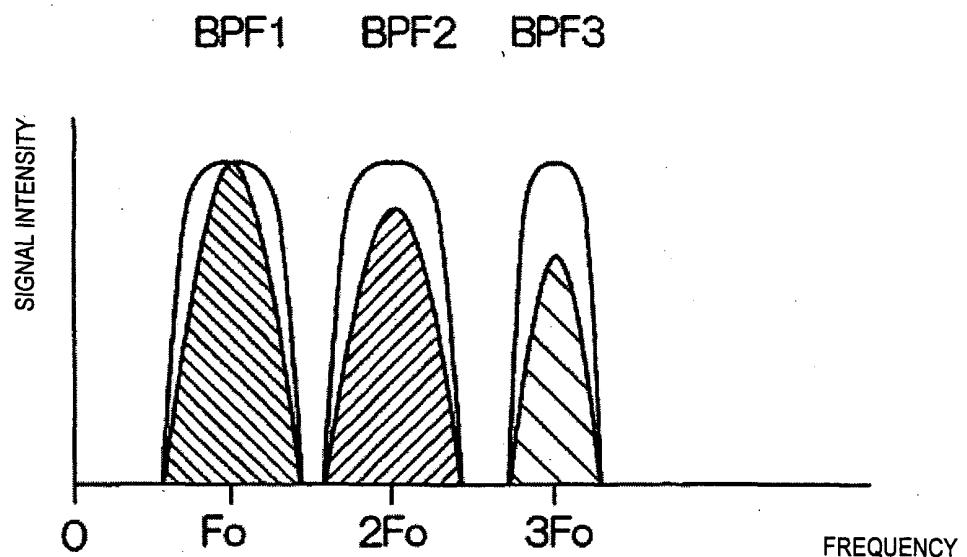


FIG.3

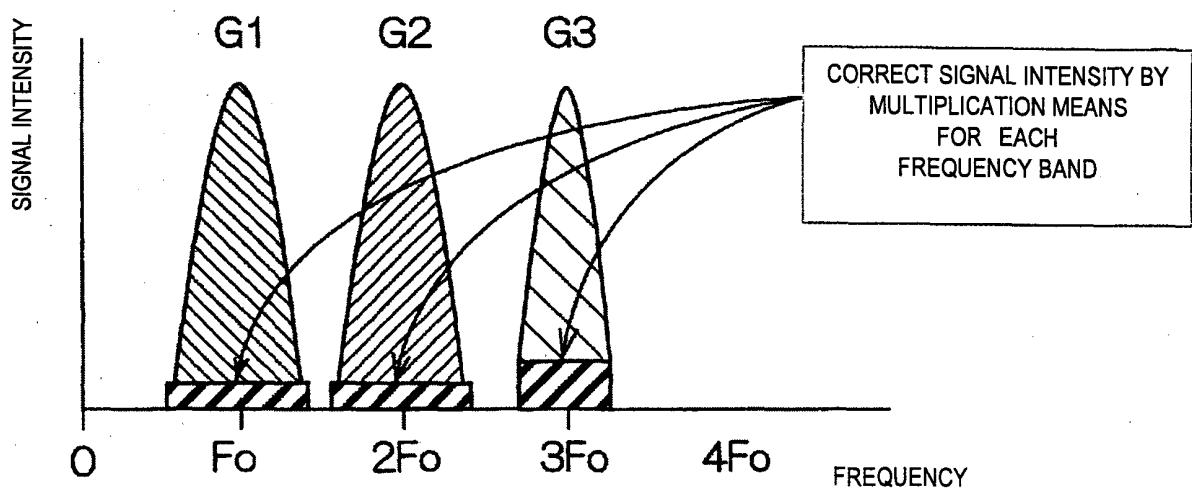


FIG.4

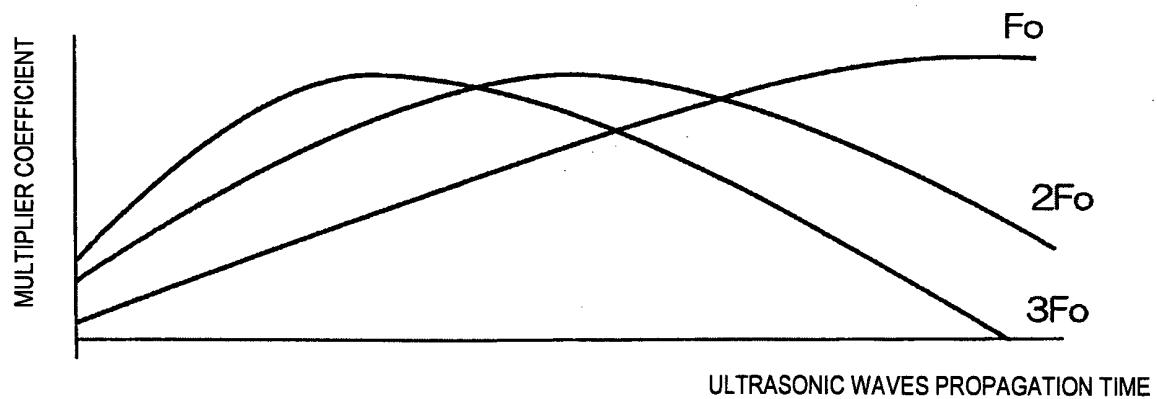


FIG.5

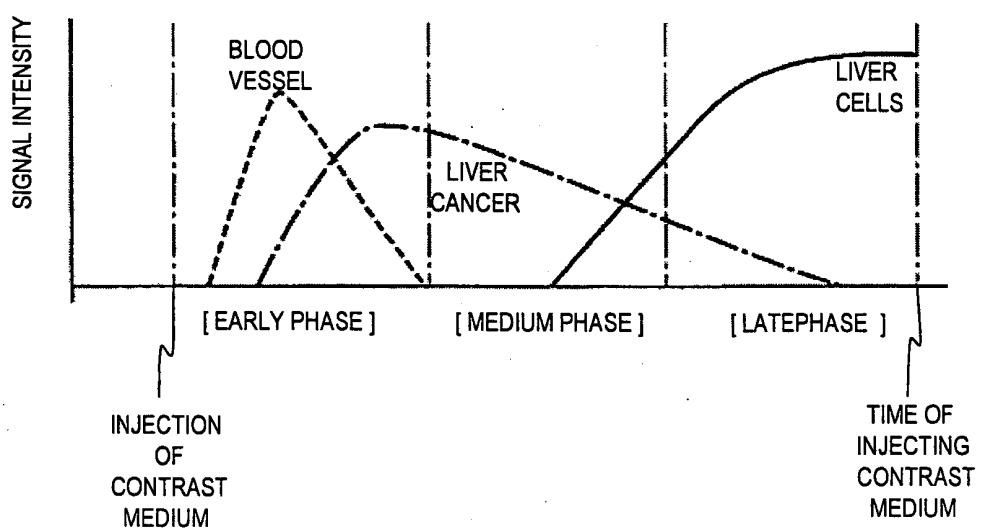


FIG.6

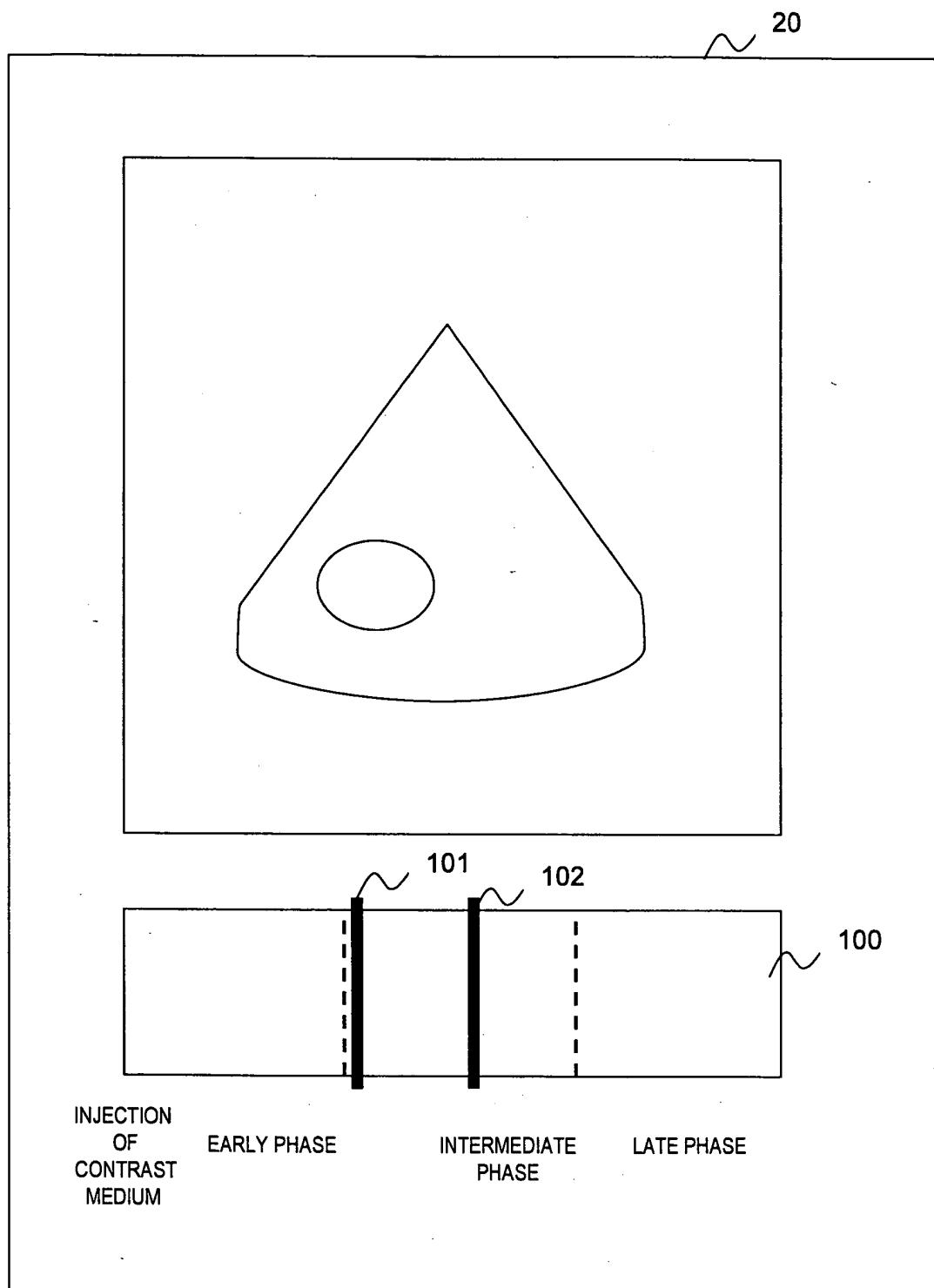
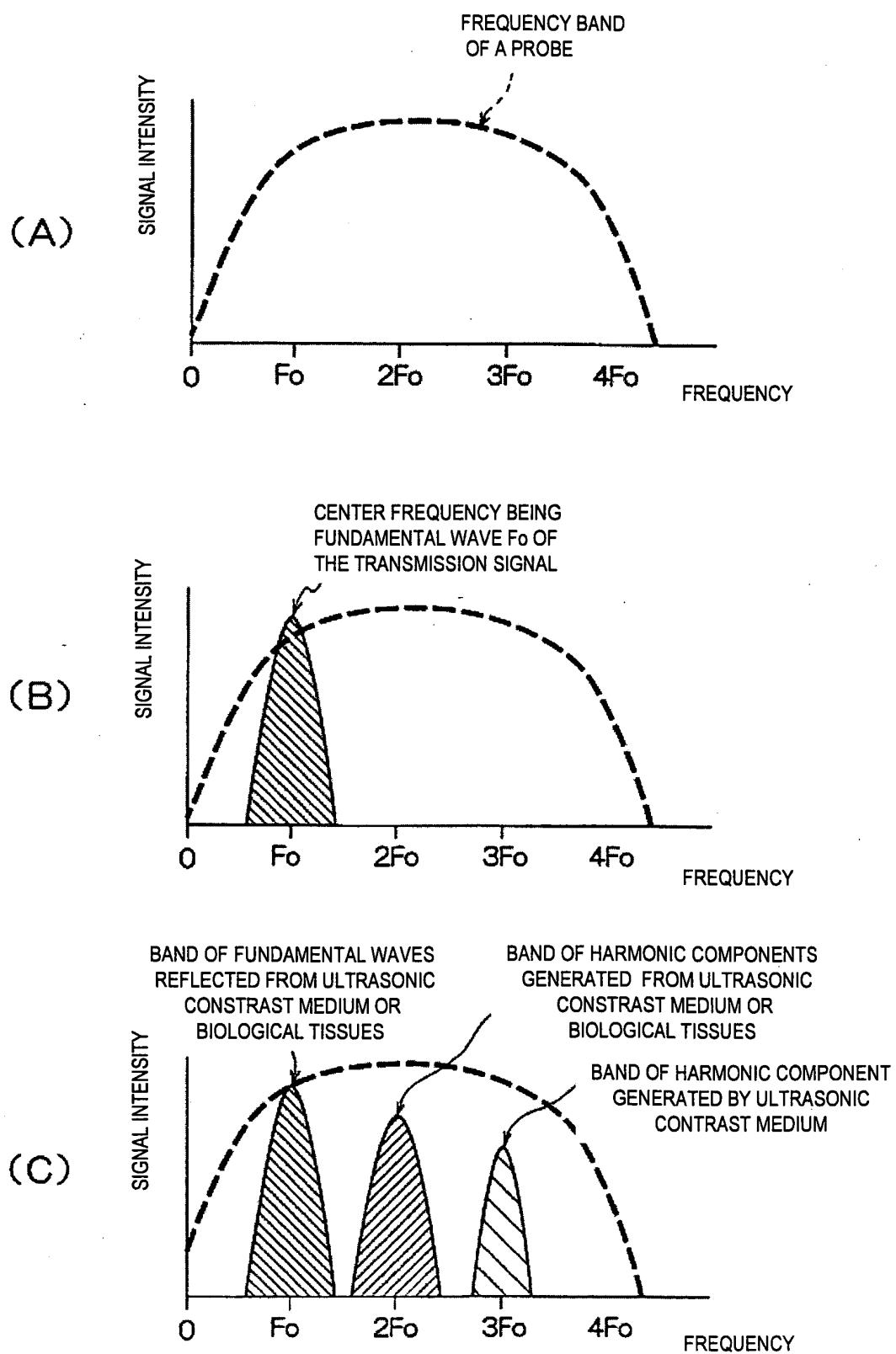


FIG. 7



INTERNATIONAL SEARCH REPORT

International application No.

PCT/JP2006/310580

A. CLASSIFICATION OF SUBJECT MATTER
A61B8/00 (2006.01) i

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)
A61B8/00

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched
Jitsuyo Shinan Koho 1922-1996 Jitsuyo Shinan Toroku Koho 1996-2006
Kokai Jitsuyo Shinan Koho 1971-2006 Toroku Jitsuyo Shinan Koho 1994-2006

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	JP 11-76231 A (Toshiba Corp.), 23 March, 1999 (23.03.99), (Family: none)	1-19
A	JP 2002-360569 A (Toshiba Corp.), 17 December, 2002 (17.12.02), (Family: none)	1-19
A	JP 2005-95376 A (GE Medical Systems Global Technology Co. LLC.), 14 April, 2005 (14.04.05), (Family: none)	1-19
A	JP 2004-208918 A (Hitachi Medical Corp.), 29 July, 2004 (29.07.04), (Family: none)	1-19

Further documents are listed in the continuation of Box C. See patent family annex.

* Special categories of cited documents:	
"A"	document defining the general state of the art which is not considered to be of particular relevance
"E"	earlier application or patent but published on or after the international filing date
"L"	document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)
"O"	document referring to an oral disclosure, use, exhibition or other means
"P"	document published prior to the international filing date but later than the priority date claimed
"T"	later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
"X"	document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
"Y"	document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art
"&"	document member of the same patent family

Date of the actual completion of the international search
18 August, 2006 (18.08.06)

Date of mailing of the international search report
29 August, 2006 (29.08.06)

Name and mailing address of the ISA/
Japanese Patent Office

Authorized officer

Facsimile No.

Telephone No.

Form PCT/ISA/210 (second sheet) (April 2005)

INTERNATIONAL SEARCH REPORT		International application No. PCT/JP2006/310580
C (Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT		
Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	JP 2002-238900 A (Aloka Co., Ltd.), 27 August, 2002 (27.08.02), (Family: none)	1-19

Form PCT/ISA/210 (continuation of second sheet) (April 2005)

INTERNATIONAL SEARCH REPORT

International application No. PCT/JP2006/310580
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Box No. II Observations where certain claims were found unsearchable (Continuation of item 2 of first sheet)

This international search report has not been established in respect of certain claims under Article 17(2)(a) for the following reasons:

1. Claims Nos.: 20

because they relate to subject matter not required to be searched by this Authority, namely:

The invention as set forth in the above claim is deemed to be concerned with diagnostic methods to be practiced on the human body. Consequently, the invention as set forth in the above claim relates to a subject matter which this International Searching Authority (continued to extra sheet)

2. Claims Nos.:

because they relate to parts of the international application that do not comply with the prescribed requirements to such an extent that no meaningful international search can be carried out, specifically:

3. Claims Nos.:

because they are dependent claims and are not drafted in accordance with the second and third sentences of Rule 6.4(a).

Box No. III Observations where unity of invention is lacking (Continuation of item 3 of first sheet)

This International Searching Authority found multiple inventions in this international application, as follows:

1. As all required additional search fees were timely paid by the applicant, this international search report covers all searchable claims.

2. As all searchable claims could be searched without effort justifying an additional fee, this Authority did not invite payment of any additional fee.

3. As only some of the required additional search fees were timely paid by the applicant, this international search report covers only those claims for which fees were paid, specifically claims Nos.:

4. No required additional search fees were timely paid by the applicant. Consequently, this international search report is restricted to the invention first mentioned in the claims; it is covered by claims Nos.:

Remark on Protest

the

- The additional search fees were accompanied by the applicant's protest and, where applicable, payment of a protest fee..
- The additional search fees were accompanied by the applicant's protest but the applicable protest fee was not paid within the time limit specified in the invitation.
- No protest accompanied the payment of additional search fees.

Form PCT/ISA/210 (continuation of first sheet (2)) (April 2005)

INTERNATIONAL SEARCH REPORT

International application No. PCT/JP2006/310580
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Continuation of Box No.II-1 of continuation of first sheet(2)

is not required, under the provisions of Article 17(2)(a)(i) of the PCT and Rule 39.1(iv) of the Regulations under the PCT, to search.

REFERENCES CITED IN THE DESCRIPTION

This list of references cited by the applicant is for the reader's convenience only. It does not form part of the European patent document. Even though great care has been taken in compiling the references, errors or omissions cannot be excluded and the EPO disclaims all liability in this regard.

Patent documents cited in the description

- JP H1176231 A [0003]

Non-patent literature cited in the description

- Capacitive Micromachined Ultrasonic Transducer: IEEE Trans, Ultrason. Ferroelect. Freq. Contro., May 1998, vol. 45, 678-690 [0011]
- *IEEE Ultrasonics Symposium*, 1996, 1451 [0032]

专利名称(译)	超声波和超声波图像显示方法		
公开(公告)号	EP1884195A1	公开(公告)日	2008-02-06
申请号	EP2006746909	申请日	2006-05-26
[标]申请(专利权)人(译)	株式会社日立医药		
申请(专利权)人(译)	日立医疗器械股份有限公司		
当前申请(专利权)人(译)	日立医疗器械股份有限公司		
[标]发明人	ASAUSA KATSUNORI HITACHI MEDICAL CORP LTD		
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IPC分类号	A61B8/00 G01S7/52		
CPC分类号	G01S7/52039 A61B8/481 G01S7/52038		
优先权	2005155835 2005-05-27 JP		
其他公开文献	EP1884195A4		
外部链接	Espacenet		

摘要(译)

提供了一种超声波诊断装置以及超声波图像显示方法，该超声波诊断装置优先用于根据来自造影剂的信号和来自生物体组织的信号生成更鲜明的图像。该超声波诊断装置包括：超声波探头10，其向被检体发送超声波；发送单元12，其向超声波探头10提供驱动信号；接收单元，其接收从超声波探头10输出的接收信号；处理装置16，用于处理从接收装置14输出的接收信号；图像处理装置18，用于根据从信号处理装置16输出的信号构造超声波图像；以及显示装置，用于显示超声波图像。信号处理装置16具有用于对于每个频带检测从接收装置14输出的接收信号的信号强度和随时间的变化量的装置。图像处理装置18具有用于区分源自造影剂的超声图像的信号和源自生物组织的信号的装置。对于每个频带，检测通过向对象发送/接收超声波而获得的接收信号的信号强度和随时间的变化量，来自造影剂和生物组织的信号基于每个频带的信号强度和时间变化量，并显示超声图像。

FIG.7

