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(54) **ULTRASONIC IMAGING DEVICE AND SYSTEM**

VORRICHTUNG UND SYSTEM ZUR ULTRASCHALLBILDGEBUNG

DISPOSITIF D'IMAGERIE PAR ULTRASONS ET SYSTEME

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Description

BACKGROUND OF THE INVENTION

1. Field of the Invention

[0001] The present invention relates to apparatus used for ultrasonic imaging. More particularly, it relates to apparatus for simultaneous imaging in both longitudinal and transverse views. More specifically, it relates to apparatus for imaging for purposes of medical diagnosis and treatment, especially for diagnosis and treatment of organs such as the prostate.

2. Prior Art

[0002] There are various situations in which it is necessary to do ultrasonic imaging to assist in medical diagnosis and treatment. For example, prostate cancer is one of the most common cancers found in men. Treatment options include "watchful waiting", hormonal therapy, brachytherapy, or surgery. Three types of surgery are used. The classical "open" procedure, radical prostatectomy, and the newly developed laproscopic and cryosurgery procedures. All procedures have risks. Both the open procedures and the laproscopic procedures have significant risks of causing impotence and incontinence. With both brachytherapy, and cryosurgery the prostate is left in vivo, and therefore the risk of complications is much lower, and the recovery time is quicker.

[0003] In brachytherapy, trains of seeds are implanted in rows in the prostate. Cryosurgery is done in a similar fashion, except that cooling needles are inserted in eight to twelve locations in the prostate. Cold gases are circulated through the needles, and the prostate is monitored by ultrasound imaging for the formation of ice balls, which indicates proper operation of the device. Both of these procedures may be preformed under local anesthetic.

[0004] As illustrated in Fig. 1, ultrasound guidance is used in order to properly locate the needle holding the seeds for brachytherapy or the needles for cryosurgery. In Fig. 1, those skilled in the art will recognize the following bladder B, prostate P, urethra U, rectum R, perianal wall Pe, operator 10, ultrasonic probe 12, needle grid block 14, needle 16, needle core 18, and seeds 20.

[0005] As illustrated in Fig. 2, in the prior art, the typical bi-plane ultrasonic probe 22 used has a linear transducer array 24 to image the sagittal or longitudinal view, and a micro-convex curved array 26 for the transverse view. The linear array is usually 50 mm long, and is not long enough to visualize the entire prostate in many patients.

[0006] As illustrated in Fig. 3, the micro-convex array 26 is at the end of the probe, and its imaging plane 28 does not intersect the linear array's imaging plane 30. This causes the operator to have to constantly move the probe to different positions along the rectum during the procedure. This is time consuming, and more importantly, causes the prostate to move, leading to more uncer-

tainty as to where the seeds are being placed.

[0007] Document US5891039 discloses an ultrasonic probe, which is formed by three integral transducers, i.e. a first, central transducer for scanning an artery axially and two lateral, further transducers, which are arranged parallel to one another and oriented perpendicularly to the first transducer in order to form transversal sectional images of the artery.

[0008] Further, document US6014473 discloses an ultrasonic imaging system, which includes an ultrasonic transducer having an image data array and a tracking array at each end of the image data array. The tracking arrays are oriented transversely to the image data array. Images from the image data array are used to reconstruct a three- dimensional representation of the target.

SUMMARY OF THE INVENTION

[0009] It is an object of the invention to provide an ultrasonic probe that allows the entire prostate to be visualized at once.

[0010] It is a further object of the invention to provide an ultrasonic probe that may be used to place the transverse scan in the middle of the prostate, thus eliminating the need to change the longitudinal position of the transducer along the rectum, and requiring rotation, which does not move the prostate significantly.

[0011] It is yet another object of the invention to allow for more accurate and quicker needle placement for brachytherapy and cryosurgery when using a standard brachytherapy and cryosurgery apparatus.

[0012] It is still another object of the invention to provide an ultrasonic probe that allows for the entire prostate to be imaged simultaneously in both longitudinal and transverse views.

[0013] These objects and others are achieved in accordance with the invention by providing a bi-plane transducer where three independent arrays are mounted, as defined in the independent claim 1. Preferred embodiments are defined in the dependent claims. There are two curved arrays typically subtending 30 degrees of arc of typically 60 mm radius mounted longitudinally on the housing, with a micro-convex array of typically 10 mm radius mounted transversely between the two larger curved arrays.

[0014] The ultrasound system used with this ultrasonic probe can be used scan all three arrays sequentially. The two convex arrays are used to create one continuous image of the longitudinal plane. The micro-convex transducer images the transverse plane. Both images can be displayed simultaneously on the system monitor. At least one high voltage multiplexer integrated circuit may be built into the handle to switch the system electronics between the three different arrays of the probe. At least one additional multiplexer may be used to switch between the above mentioned probe and another probe.

BRIEF DESCRIPTION OF THE DRAWINGS

[0015] The foregoing aspects and other features of the present invention are explained in the following description, taken in connection with the accompanying drawings, wherein:

Fig. 1 is a cross-sectional view of a patient with an ultrasonic probe in the rectum held in a brachytherapy device, and with an additional imaging probe.

Fig. 2 is a perspective view of a prior art ultrasonic probe with a prior art transducer assembly.

Fig. 3 illustrates the scan planes of the prior art device of Fig. 1.

Fig. 4 is a perspective view of the operative end of an ultrasonic probe in accordance with the invention.

Fig. 5 is a cross sectional view of the embodiment of the invention illustrated in Fig. 4.

Fig. 6 illustrates the scan planes of the ultrasonic probe in accordance with the invention.

Fig. 7 is block diagram of a system using the ultrasonic probes, in accordance with the invention.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENT

[0016] Referring again briefly to Fig. 1, in accordance with the invention, an additional ultrasonic imaging probe 19 may be placed on the abdominal wall of the patient 21 to image the prostate P from above. Probe 19 may have an array of, for example 128 transducers, in a flat or slightly concave configuration, and thus may be suited to image structures through the abdominal wall of the patient. The coordination of images produced by ultrasonic probe 42 and probe 19 is explained below with respect to Fig. 7. Due to the location of probe 19, with the consequent need for the ultrasound produced and received by probe 19 to traverse a larger distance to and from the prostate than the ultrasound from probe 42, probe 19 may operate at a frequency lower than that used to excite the elements of the transducers of probe 42, or, in some applications, at the same frequency.

[0017] Referring to Fig. 4, there is shown a perspective view of the operative or distal end portion 40 of an ultrasonic probe 42 incorporating features of the present invention. Although the present invention will be described with reference to the single embodiment shown in the drawings, it should be understood that the present invention can be embodied in many alternate forms of embodiments. In addition, any suitable size, shape or type of elements or materials could be used.

[0018] Referring also to Fig. 5, ultrasonic probe 42 in-

cludes a substantially hollow probe housing 44 having a handle 46, a flexible cable guide 47 for a multi-wire cable (not shown in Fig. 5) a connecting tube 48, and end portion 40. These components (except for cable guide 47) may be constructed of a high strength engineering plastic, which retains its properties after multiple exposures to the heat required for cleaning and sterilization. End portion 40 has a solid insert 49, formed of an insulating material, and designed to support appropriate connecting wires (not shown) and three transducer arrays, as described below.

[0019] The three transducer arrays of end portion 40 are for emitting and receiving ultrasound for the purpose of imaging the organs of a patient, and in particular, the prostate of a patient. These transducer arrays include a first convex array 50, a second convex array 52, and a micro-convex array 54.

[0020] Transducer arrays 50 and 52 may each comprise 96 piezoelectric elements, having a pitch of 0.327 mm, an elevation of 5 mm, and a focal distance of 30 mm. Each array may subtend 30 degrees of arc, of a 60 mm radius of curvature. The frequency of resonance of the piezoelectric elements may be 6.5 MHz.

[0021] Micro-convex transducer array 54 may include 128 elements. Alternatively, it may include 96 elements on a pitch of 0.215 mm, having an elevation of 5 mm and a focal distance of 30 mm, with the beam formed subtending an angle of 180 degrees. The frequency of resonance of the piezoelectric elements may be 6.5 MHz.

[0022] As noted above, multiplexing electronics may be located in handle 46 of housing 44. A cable (not shown in Fig. 5) having a 156 pin connector, such as a Cannon ZIF connector, may be used to connect the electronics to an electronics module (Fig. 7) so that images may be generated and viewed.

[0023] Fig. 6 illustrates the relationship between the sagittal or longitudinal scan planes 60 and 62 generated by arrays 50 and 52 respectively, and the transverse scan 64 generated by micro-convex curved array 54. It is noted that scan planes 60 and 62 are co-planar and partially overlap, thus permitting the entire prostate to be imaged along a single longitudinal plane without moving probe 42 in the rectum of the patient. Micro-convex transducer array 54 provides an image in a transverse scan plane 64 that is perpendicular to scan planes 60 and 62. The location of transducer array 54 between transducer arrays 50 and 52 means that the center of the prostate may be imaged in the transverse plane at the same time as the entire prostate is imaged in the longitudinal plane. In other words, the transducer arrays are aligned, or positioned with respect to one another, so that the transverse imaging array produces an image at (or in the general case, near) the center of the longitudinal image.

[0024] Referring to Fig. 7, ultrasonic transducer 19 and ultrasonic probe 42 are connected to an electronics module 100, which contains the circuitry necessary to excite the ultrasonic transducer 19 and ultrasonic probe 42 so as to send pulses of ultrasound into the patient, receive

ultrasound reflected from internal structures and organs, and convert the signals, in a desired fashion to an image or images which may be interpreted in a medically significant fashion. In general, such modules are well known in the art. However, the use of ultrasonic transducer 19 and ultrasonic probe 42 gives rise to a unique arrangement of components.

[0025] In general, module 100 may be controlled by a microprocessor 102 connected by suitable lines 103 to a control input 104. Microprocessor 102 and control input 104 may be dedicated, hardwired components (such as a control panel with appropriate switches and knobs for control input 104) within module 100, or may represent, for example a personal computer and a keyboard, respectively, interfaced in a manner well known in the art to the remainder of module 100. If this is the case, suitable software may be provided to allow the keyboard to provide the control inputs typically provided in a module 100, such as brightness, contrast, color control, and control over parameter such as frequency of operation, focus, beam steering, system gain, and other necessary parameters, as more fully described below. In a like manner, a video processor 106 and a display 108 may also be dedicated components of the module 100 or the video driver card and monitor of the personal computer.

[0026] Frequency control inputs provided by control input 104 are processed by microprocessor 102 and provided in suitable form to a frequency control 110. An output of frequency control 110 determines the rate at which entries in a table memory 112 are read out to each of sixty-four different transmitter channels represented as 114. Table memory 112 includes a multidimensional array of waveform values. The values that are read out for one of the dimensions is determined by a depth control 116, in response to inputs from microprocessor 102, as determined by input from control input 104. Thus the depth of display desired may be adjusted.

[0027] The outputs of the transmitter channels are supplied to a transmit/receive switch 118, which is in turn connected to a 4:1 multiplexer or MUX 120 and sixty-four receiver channels, as represented by 122. The transmit/receive switch 118 serves to switch the sixty-four inputs of 4:1 MUX 120 between transmitter channels 114 and receiver channels 122 in a manner well known in the art.

[0028] The 4:1 MUX 120 serves to switch the 64 transmitter and receiver channels between 128 elements of transducer 19 (sixty four elements at a time) and the 96 elements of one of the transducer arrays of ultrasonic probe 42. In other words, there are 256 outputs on one side of MUX 120 (the side connected to the cables to transducer 19 and probe 42) and 64 on the other side connected to transmit/receive switch 118. However, in the case of probe 42, some of the outputs are not used. MUX 120 may be a high voltage, low impedance switching multiplexer, such as that manufactured by Supertex, Inc., located in Sunnyvale, CA, USA.

[0029] A second multiplexer or MUX 124 (in this case a 3:1 multiplexer located in the handle of probe 42) having

128 ports on each side, is used to successively connect 96 outputs of MUX 120 to the respective element of the three transducer element arrays of probe 42 described above. MUX 124 may be of the same general type as MUX 120.

[0030] Receiver channels 122 provide suitable amplification and conditioning of analog signals returned by transducer elements of transducer 19 and probe 42 in response to reflections of ultrasound by structures within the patient. Gain control signals are provided to receiver channels 122 by a bus 125. The analog signals are converted to digital form by a series of sixty-four analog-to-digital converters or A/D's 126. As is well known in the art, the number of A/D output signals used to form an image is a function of depth of the image, generally with more channels being used for imaging at greater depth. A beam steering and focusing circuit 128 processes the digital signals from the A/D's 126. The outputs of beam steering and focusing circuit 128 are provided to video processor 106 to provide a suitable representation of the patient on display 108.

[0031] Microprocessor 102 has appropriate outputs 130 and 132 for controlling MUX 120 and MUX 124, as required to perform the sequence of switching described herein.

[0032] The images provided on display 108 advantageously include those provided by the three transducer arrays of probe 42, as discussed above. In addition, an image generated by signals from probe 19 may also be displayed, preferably above the image resulting from the signals from probe 42. Thus, in addition to imaging the transverse plane and the entire longitudinal plane of an organ, such as the prostate, or a defined region, a top view may be displayed as well. The various images, when taken together, provide an excellent, very precise view of the organ or image in three dimensions, allowing the precise location of structures and therefore the accurate placement of, for example, seeds or needles, for brachytherapy or cryosurgery, as described above.

[0033] It should be understood that the foregoing description is only illustrative of the invention. Accordingly, the present invention is intended to embrace all alternatives, modifications and variances which fall within the scope of the appended claims.

Claims

1. An ultrasonic probe (42) comprising:

- an elongate structure having a longitudinal axis;
- a first array of ultrasonic transducer elements (50) extending along an outer surface of said elongate structure in a direction generally parallel to said longitudinal axis so as to generate a first scan plane (60);
- a second array of ultrasonic transducer elements (52) extending along the outer surface of

- the elongate structure in a direction generally parallel to said longitudinal axis so as to generate a second scan plane (62) and a third array of ultrasonic transducer elements (54) extending about said elongate structure in a direction so that it images a plane perpendicular to that imaged by at least one of said first array and said second array, the third array being disposed in a space between said first array and said second array **characterised in that** the first scan plane and the second scan plane are configured to extend along said longitudinal axis.
2. The probe of claim 1, wherein said first array, said second array and said third array are outwardly convex arrays.
 3. The probe of claim 2, wherein said third array has a radius of curvature smaller than that of said first array and said second array.
 4. The probe of claim 2, wherein said first array and said second array have a radius of curvature of substantially 60 millimeters.
 5. The probe of claim 2, wherein said third array has a radius of curvature of substantially 10 millimeters.
 6. The probe of claim 1, wherein said first array and said second array are configured so that beams formed by said first array and said second array subtend substantially thirty degrees of arc.
 7. The probe of claim 1, wherein said third array is configured so that a beam formed by said third array subtends substantially 180 degrees of arc.
 8. The probe of claim 1, further comprising a multiplexer for multiplexing connections to each of said first array, said second array and said third array.
 9. The probe of claim 8, wherein said multiplexer is disposed within said elongate structure.
 10. The probe of claim 1, wherein said first array and said second array are aligned so as to image a portion of a substantially continuous plan perpendicular to said plane imaged by said third array.
 11. The probe of claim 1, wherein each of said first array, said second array and said third array are comprised of transducer elements having a resonant frequency of 6.5 Megahertz.
 12. The probe of claim 1, in combination with a second probe, said second probe being capable of positioning so as to imaging in a plane perpendicular to a plan imaged by said first array and a plane imaged by said second array.
 13. The combination of claim 12, wherein said second probe comprises transducer elements with a resonant frequency of 6.5 Megahertz.
 14. The probe of claim 1, in combination with an electronics module, comprising : excitation circuitry for providing excitation energy to said probe; receiving circuitry for processing signals received by said probe; signal processing circuitry for processing signals from said receiving circuitry to produced processed image signals; and a display for displaying the processed image signals.
 15. The combination of claim 14, further comprising at least one of frequency setting circuitry for setting a frequency of the excitation energy; depth control circuitry for controlling the depth of images produced on said display; gain control circuitry for controlling gain of said receiving circuitry; and steering and focus control circuitry as a component of said signal processing circuitry for controlling the manner of operation of said signal processing circuitry.
 16. The combination of claim 14, wherein said excitation circuitry comprises a table memory for providing values of waveforms used to excite transducer elements of said probe.
 17. The combination of claim 14, further comprising analog to digital converters as components of said signal processing circuitry for converting analog signals from said receiving circuitry into digital signals.

Patentansprüche

1. Ultraschallsonde (42) umfassend:

eine längliche Struktur mit einer Längsachse ;
 ein erstes Array aus Ultraschallmessfühlerelementen (50), das sich entlang einer Außenfläche der länglichen Struktur in eine im Allgemeinen parallele Richtung zur Längsachse erstreckt, um eine erste Abtastebene (60) zu erzeugen,
 ein zweites Array aus Ultraschallmessfühlerelementen (52), das sich entlang der Außenfläche der länglichen Struktur in eine im Allgemeinen parallele Richtung zur Längsachse erstreckt, um eine zweite Abtastebene (62) zu erzeugen, und
 ein drittes Array aus Ultraschallmessfühlerelementen (54), das sich entlang der länglichen Struktur in eine Richtung erstreckt, um in einer Ebene, die rechtwinklig zu der durch das erste

- und/oder zweite Array abgebildeten Ebene ist, ein Bild zu erzeugen, wobei das dritte Array in einem Zwischenraum zwischen dem ersten Array und dem zweiten Array angeordnet ist, **dadurch gekennzeichnet, dass** sich die erste Abtastebene und die zweite Abtastebene entlang der Längsachse erstrecken.
2. Sonde nach Anspruch 1, wobei das erste Array, das zweite Array und das dritte Array nach außen konvex verlaufende Arrays sind.
 3. Sonde nach Anspruch 2, wobei das dritte Array einen Krümmungsradius aufweist, der kleiner als jener des ersten Arrays und des zweiten Arrays ist.
 4. Sonde nach Anspruch 2, wobei das erste Array und das zweite Array einen Krümmungsradius von im Wesentlichen 60 Millimeter aufweisen.
 5. Sonde nach Anspruch 2, wobei das dritte Array einen Krümmungsradius von im Wesentlichen 10 Millimeter aufweist.
 6. Sonde nach Anspruch 1, wobei das erste Array und das zweite Array derart ausgebildet sind, dass sich durch das erste Array und das zweite Array gebildete Strahlen im Wesentlichen über 30 Bogensekunden erstrecken.
 7. Sonde nach Anspruch 1, wobei das dritte Array derart ausgebildet ist, dass sich ein durch das dritte Array gebildeter Strahl im Wesentlichen über 180 Bogensekunden erstreckt.
 8. Sonde nach Anspruch 1, die des Weiteren einen Multiplexer zum Multiplexen von Verbindungen an sowohl den ersten Array, den zweiten Array als auch den dritten Array umfasst.
 9. Sonde nach Anspruch 8, wobei der Multiplexer innerhalb der länglichen Struktur angeordnet ist.
 10. Sonde nach Anspruch 1, wobei das erste Array und das zweite Array derart ausgerichtet sind, dass ein Teil einer im Wesentlichen durchgehenden Ebene, die rechtwinklig zu der durch das dritte Array abgebildeten Ebene ist, abgebildet wird.
 11. Sonde nach Anspruch 1, wobei sowohl das erste Array, das zweite Array als auch das dritte Array Messfühlerelemente mit einer Resonanzfrequenz von 6,5 Megahertz umfassen.
 12. Sonde nach Anspruch 1, in Kombination mit einer zweiten Sonde, wobei die zweite Sonde derart positionierbar ist, um in einer Ebene, die rechtwinklig zu einer durch das erste Array abgebildeten Ebene und zu einer durch das zweite Array abgebildeten Ebene ist, ein Bild zu erzeugen.,
 13. Kombination nach Anspruch 12, wobei die zweite Sonde Messfühlerelemente umfasst, die eine Resonanzfrequenz von 6,5 Megahertz aufweisen.
 14. Sonde nach Anspruch 1, in Kombination mit einem Elektronikmodul, umfassend: eine Anregungsschaltung zum Versorgen der Sonde mit Anregungsenergie; eine Empfangsschaltung zum Verarbeiten von Signalen, die von der Sonde empfangen werden; Signalverarbeitungsschaltung zum Verarbeiten von Signalen von der Empfangsschaltung, um aufbereitete Bildsignale zu erzeugen; und eine Anzeige zum Anzeigen der aufbereiteten Bildsignale.
 15. Kombination nach Anspruch 14, die des Weiteren umfasst: eine Frequenzregelungsschaltung zum Einstellen der Frequenz der Anregungsenergie und/oder eine Tiefenregelungsschaltung zum Regeln der Tiefe von Bildern, die auf der Anzeige erzeugt werden und/oder eine Verstärkungsregelungsschaltung zum Regeln der Verstärkung der Empfangsschaltung und/oder eine Lenk- und Fokussierregelungsschaltung als ein Bestandteil der Signalverarbeitungsschaltung zum Regeln der Betriebsart der Signalverarbeitungsschaltung.
 16. Kombination nach Anspruch 14, wobei die Anregungsschaltung einen Tabellenspeicher zum Bereitstellen von Wellenformwerten umfasst, die zur Anregung der Messfühlerelemente der Sonde verwendet werden.
 17. Kombination nach Anspruch 14, die des Weiteren Analog-Digital-Wandler als Bestandteile der Signalverarbeitungsschaltung umfasst, um analoge Signale der Empfangsschaltung in digitale Signale umzuwandeln.

Revendications

1. Sonde à ultrasons (42) comprenant :

une structure allongée ayant un axe longitudinal ;
 une première matrice d'éléments transducteurs à ultrasons (50) s'étendant le long de la surface extérieure de ladite structure allongée dans une direction globalement parallèle audit axe longitudinal de façon à générer un premier plan de balayage (60) ;
 une deuxième matrice d'éléments transducteurs à ultrasons (52) s'étendant le long de la surface extérieure de la structure allongée dans

- une direction globalement parallèle audit axe longitudinal de façon à générer un deuxième plan de balayage (62) ; et
une troisième matrice d'éléments transducteurs à ultrasons (54) s'étendant autour de ladite structure allongée dans une direction telle à former l'image d'un plan perpendiculaire à l'image formée par au moins une matrice parmi ladite première matrice et ladite deuxième matrice, la troisième matrice étant disposée dans un espace compris entre ladite première matrice et ladite deuxième matrice,
caractérisée en ce que le premier plan de balayage et le deuxième plan de balayage sont configurés de manière à s'étendre le long dudit axe longitudinal.
2. Sonde selon la revendication 1, dans laquelle ladite première matrice, ladite deuxième matrice et ladite troisième matrice sont des matrices convexes vers l'extérieur.
 3. Sonde selon la revendication 2, dans laquelle ladite troisième matrice possède un rayon de courbure plus petit que celui de ladite première matrice et de ladite deuxième matrice.
 4. Sonde selon la revendication 2, dans laquelle ladite première matrice et ladite deuxième matrice ont un rayon de courbure sensiblement de 60 mm.
 5. Sonde selon la revendication 2, dans laquelle ladite troisième matrice possède un rayon de courbure sensiblement de 10 mm.
 6. Sonde selon la revendication 1, dans laquelle ladite première matrice et ladite deuxième matrice sont configurées de telle sorte que les faisceaux formés par ladite première matrice et ladite deuxième matrice sous-tendent sensiblement un arc de 30°.
 7. Sonde selon la revendication 1, dans laquelle ladite troisième matrice est configurée de façon que le faisceau formé par ladite troisième matrice sous-tende sensiblement un arc de 180°.
 8. Sonde selon la revendication 1, comprenant en outre un multiplexeur pour multiplexer des connexions vers chaque matrice parmi ladite première matrice, ladite deuxième matrice et ladite troisième matrice.
 9. Sonde selon la revendication 1, dans laquelle ledit multiplexeur est disposé à l'intérieur de ladite structure allongée.
 10. Sonde selon la revendication 1, dans laquelle ladite première matrice et ladite deuxième matrice sont alignées de telle sorte à former l'image d'une partie d'un plan sensiblement continu perpendiculaire audit plan dont l'image est formée par ladite troisième matrice.
 11. Sonde selon la revendication 1, dans laquelle chaque matrice parmi ladite première matrice, ladite deuxième matrice et ladite troisième matrice est constituée d'éléments transducteurs ayant une fréquence de résonance de 6,5 MHz.
 12. Sonde selon la revendication 1, en combinaison avec une deuxième sonde, ladite deuxième sonde étant capable d'être positionnée de façon à former l'image dans un plan perpendiculaire à un plan dont l'image est formée par ladite première matrice et un plan dont l'image est formée par ladite deuxième matrice.
 13. Combinaison selon la revendication 12, dans laquelle ladite deuxième sonde comprend des éléments transducteurs avec une fréquence de résonance de 6,5 MHz.
 14. Sonde selon la revendication 1, en combinaison avec un module électronique, comprenant : des circuits d'excitation pour fournir une énergie d'excitation à ladite sonde ; des circuits de réception pour traiter les signaux reçus par ladite sonde ; des circuits de traitement de signal pour traiter les signaux provenant desdits circuits de réception pour produire des signaux d'images traités ; et un dispositif d'affichage pour afficher les signaux d'images traités.
 15. Combinaison selon la revendication 14, comprenant en outre au moins des circuits parmi des circuits de détermination de fréquence pour déterminer la fréquence de l'énergie d'excitation ; des circuits de commande de profondeur pour commander la profondeur des images produites sur ledit dispositif d'affichage ; des circuits de commande de gain pour commander le gain desdits circuits de réception ; et des circuits de direction et de focalisation en tant que composant dudit circuit de traitement de signal pour commander la manière de fonctionner desdits circuits de traitement de signal.
 16. Combinaison selon la revendication 14, dans laquelle lesdits circuits d'excitation comprennent une mémoire de table pour fournir des valeurs de forme d'onde utilisées pour exciter les éléments transducteurs de ladite sonde.
 17. Combinaison selon la revendication 14, comprenant en outre des convertisseurs analogique-numérique en tant que composants desdits circuits de traitement de signal pour convertir en signaux numériques des signaux analogiques provenant desdits circuits de réception.

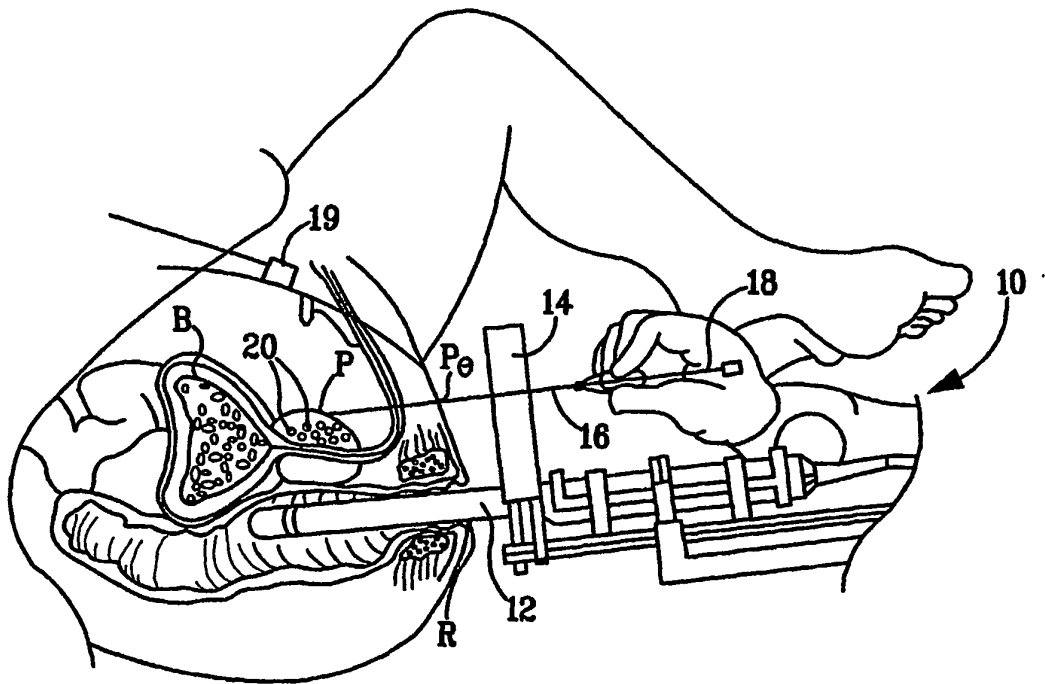


FIG. 1
Prior Art

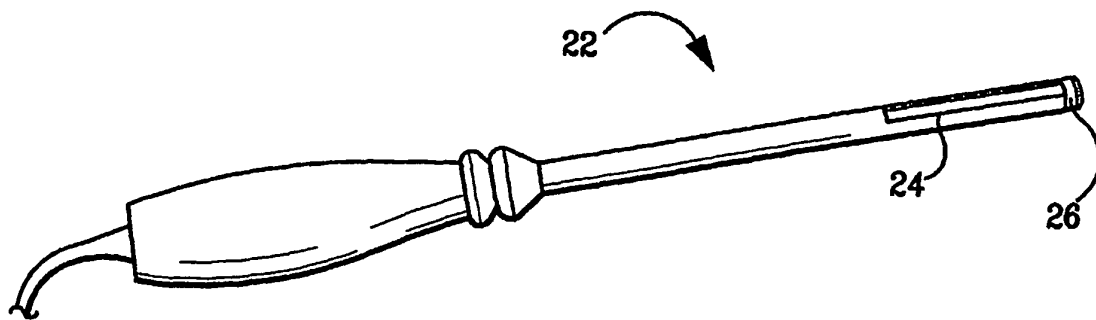


FIG. 2
Prior Art

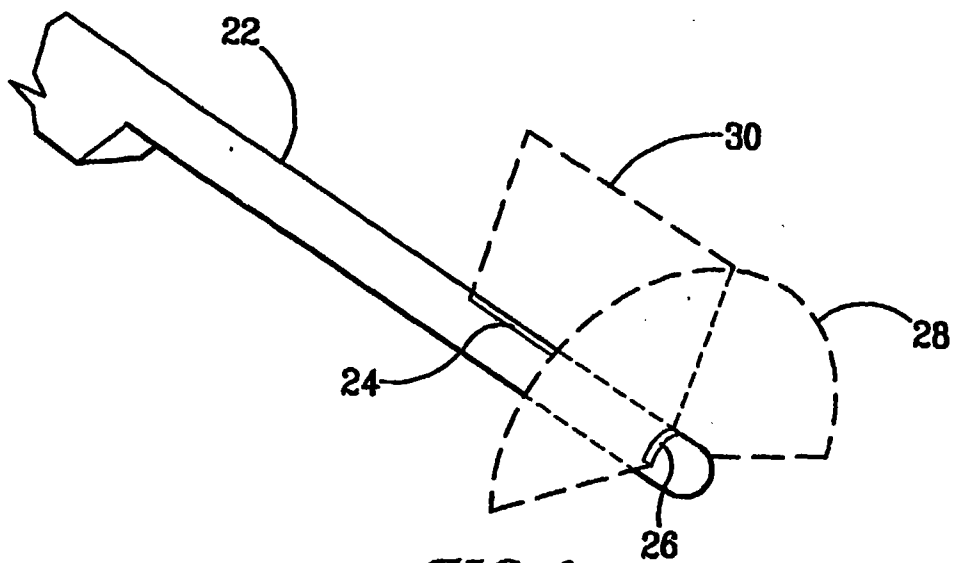


FIG. 3
Prior Art

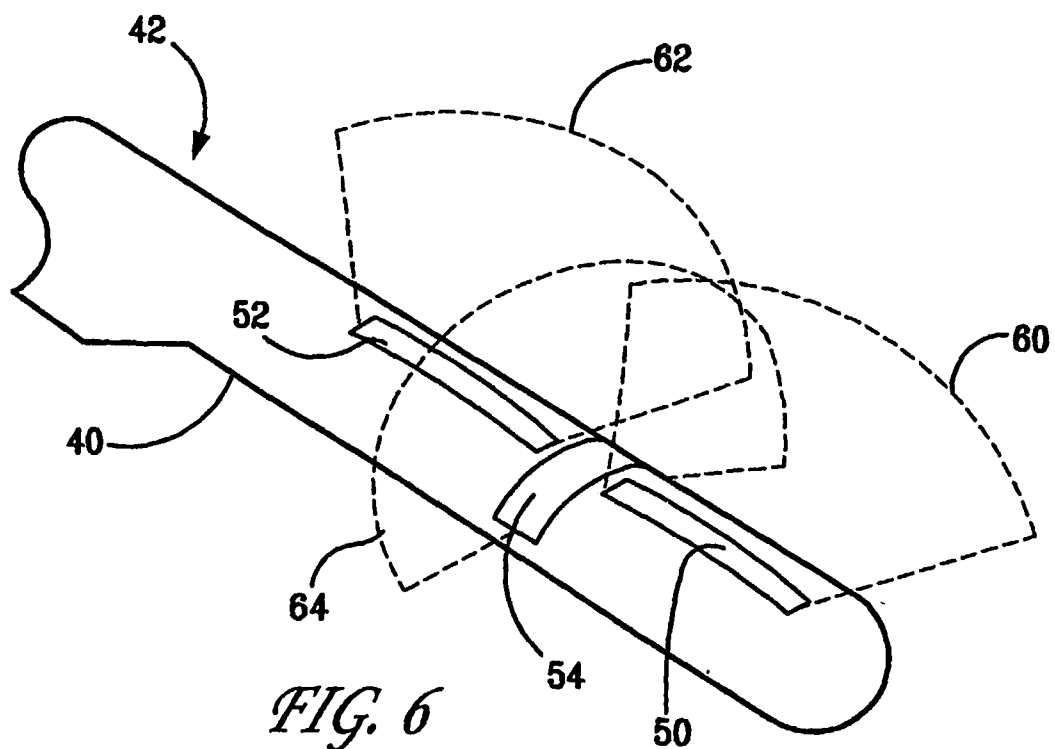
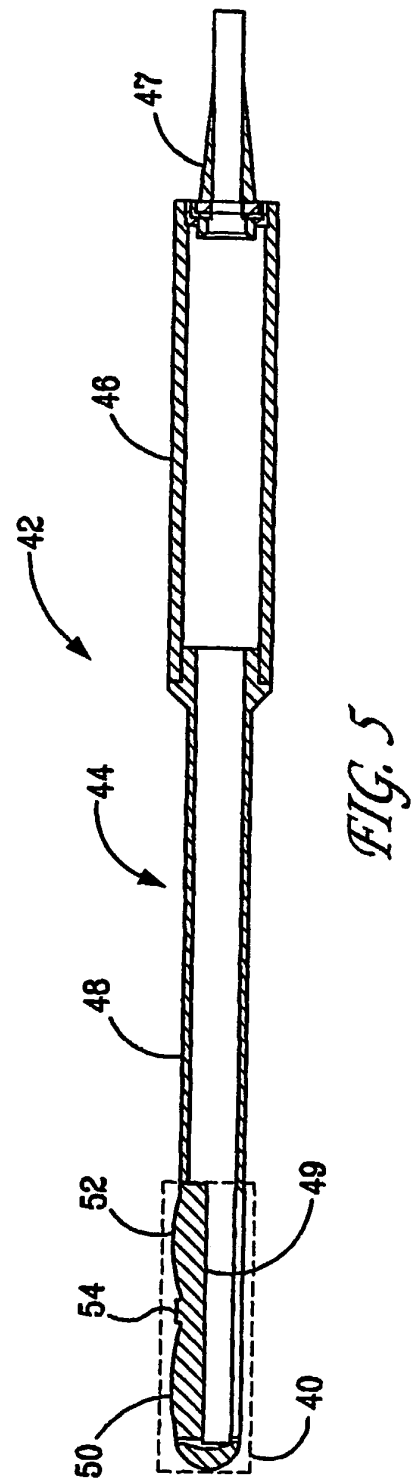
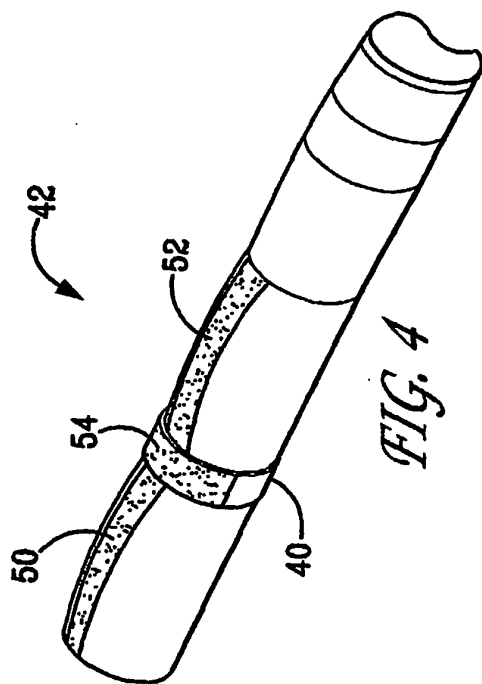


FIG. 6



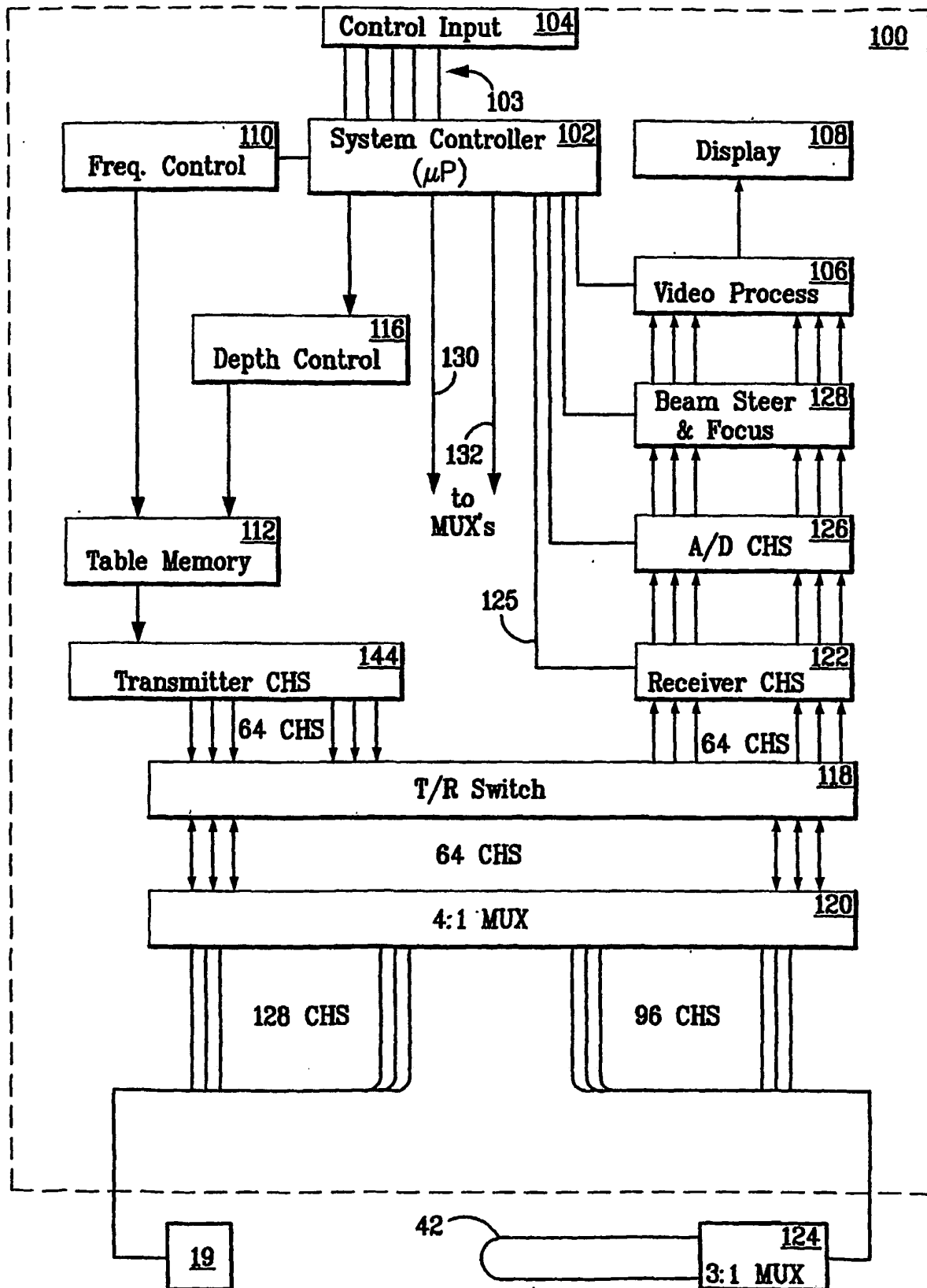


FIG. 7

REFERENCES CITED IN THE DESCRIPTION

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Patent documents cited in the description

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摘要(译)

超声波探头包括具有纵向轴线的细长结构;超声换能器元件的第一阵列沿细长结构的外表面沿大致平行于纵向轴线的方向延伸;第二阵列的超声波换能器元件沿着细长结构的外表面沿大致平行于纵向轴线的方向延伸;第三阵列超声换能器元件在一个方向上围绕细长结构延伸，使得它成像垂直于由第一阵列和第二阵列中的至少一个成像的平面，第三阵列设置在第一阵列和第二阵列之间的空间中数组和第二个数组。用于探针的电子模块和附加探针，以产生患者的内部图像。