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(54) **ANALOG CANCELLATION OF MRI SEQUENCING NOISE APPEARING IN AN ECG SIGNAL**

(52) **U.S. Cl.**  
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(57) **ABSTRACT**

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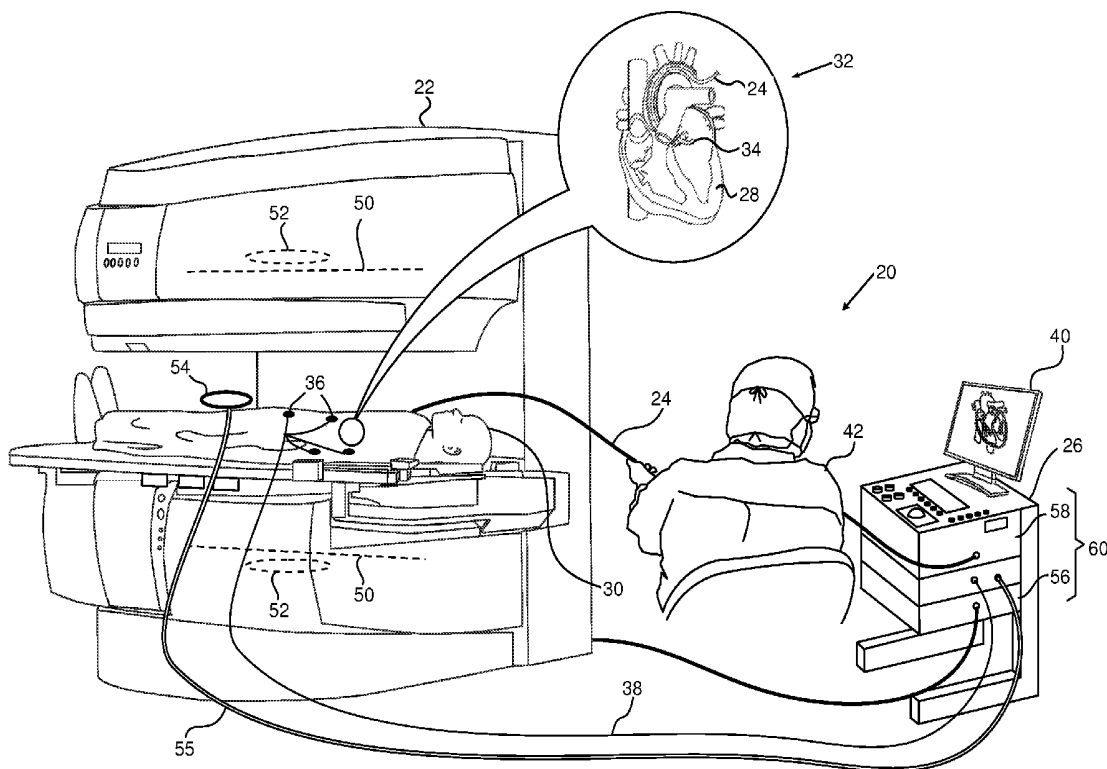
A method, including, while imaging a patient using an initial magnetic resonance imaging (MRI) sequence, generating an initial MRI reference signal in response to the initial MRI sequence using a reference sensor placed in proximity to the patient. The method further includes identifying, by locking on to the initial MRI reference signal, noise that will be generated in electrocardiograph (ECG) signals received from the patient, and computing a programmable correction to be applied to the ECG signals to reduce the noise. The method also includes applying the programmable correction to reduce the noise in the ECG signals, received from the patient, while imaging the patient using a subsequent MRI sequence and while locking on to a subsequent MRI reference signal generated in response to the subsequent MRI sequence using the reference sensor.

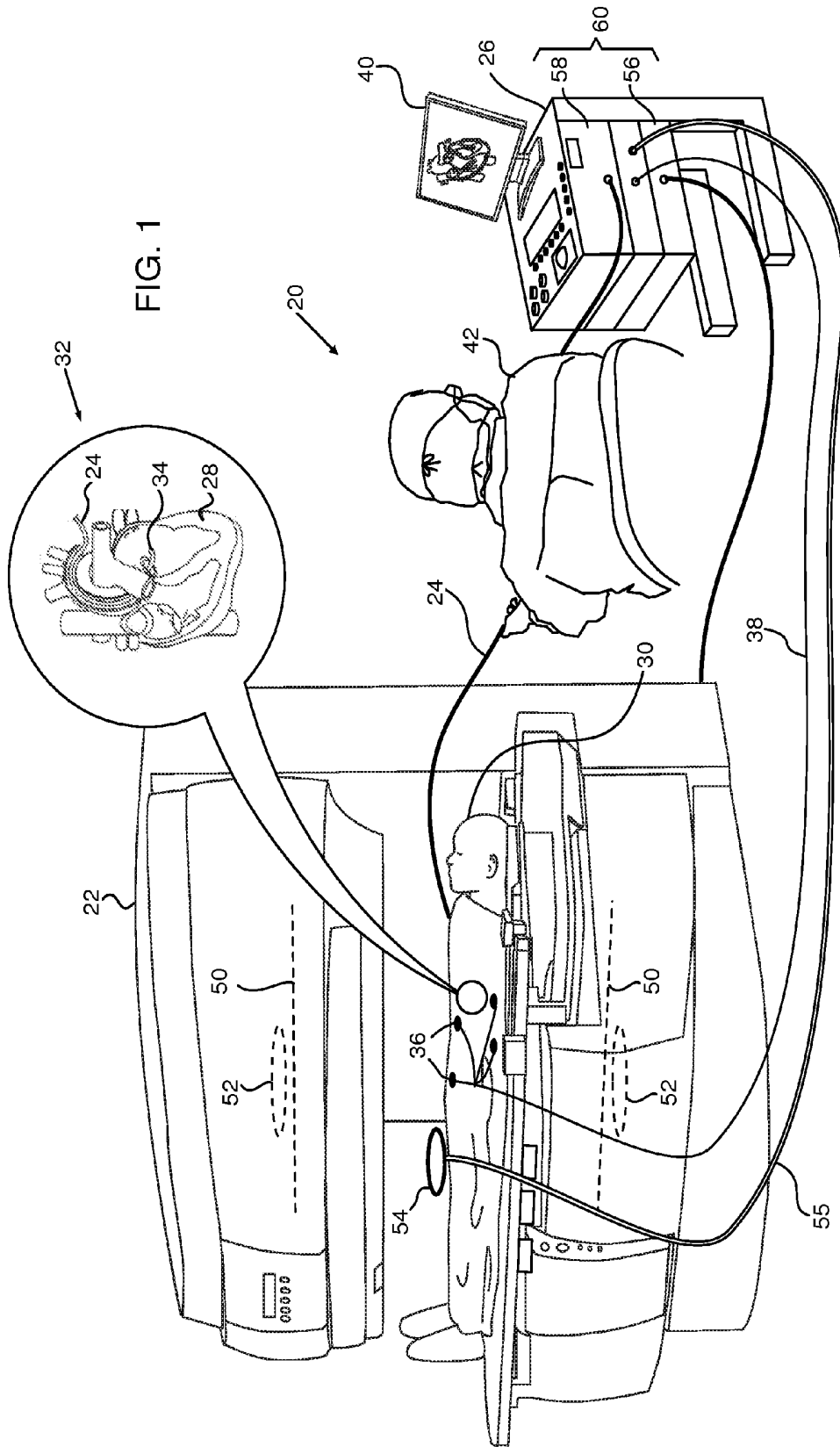
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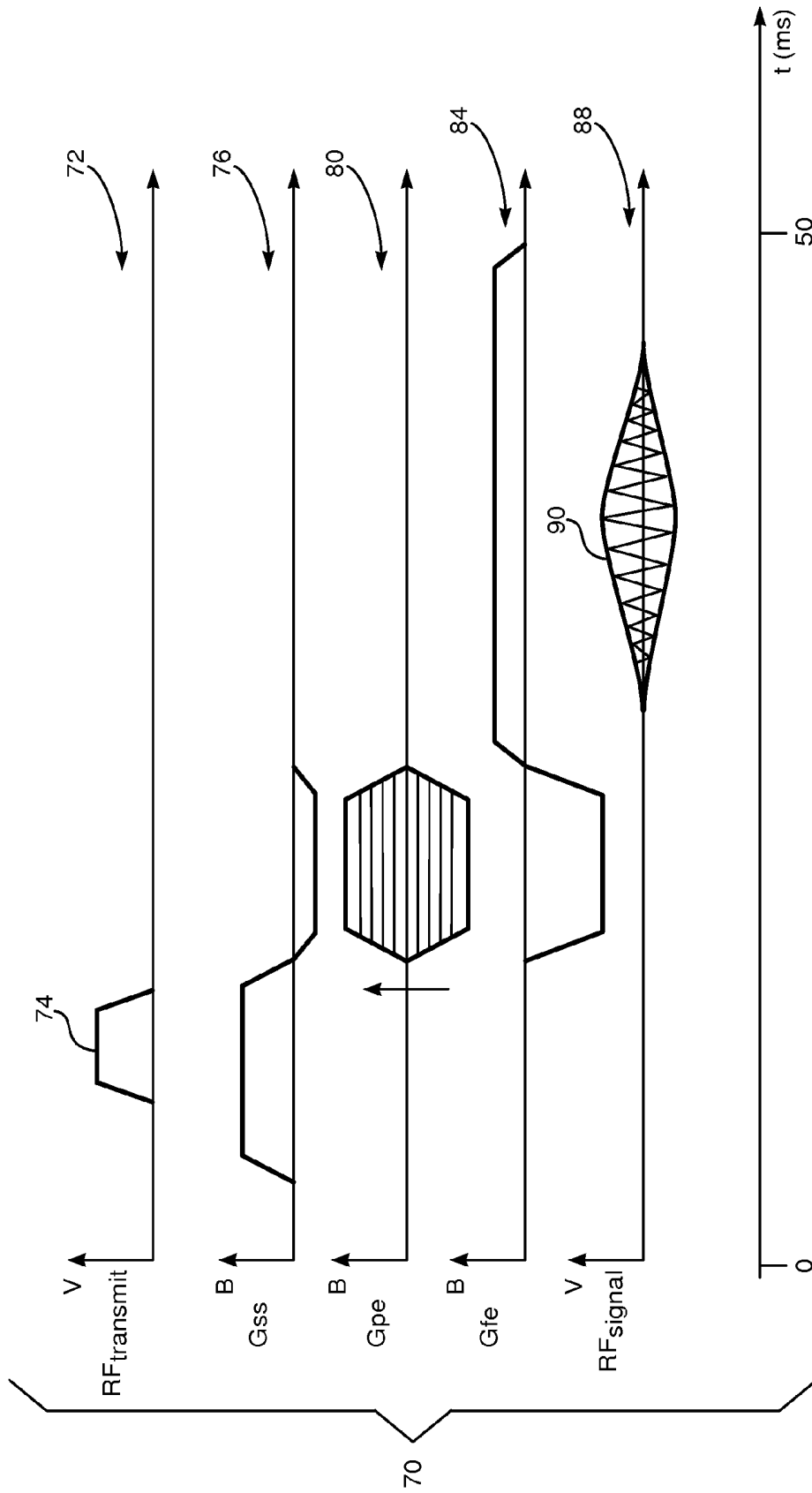


FIG. 2

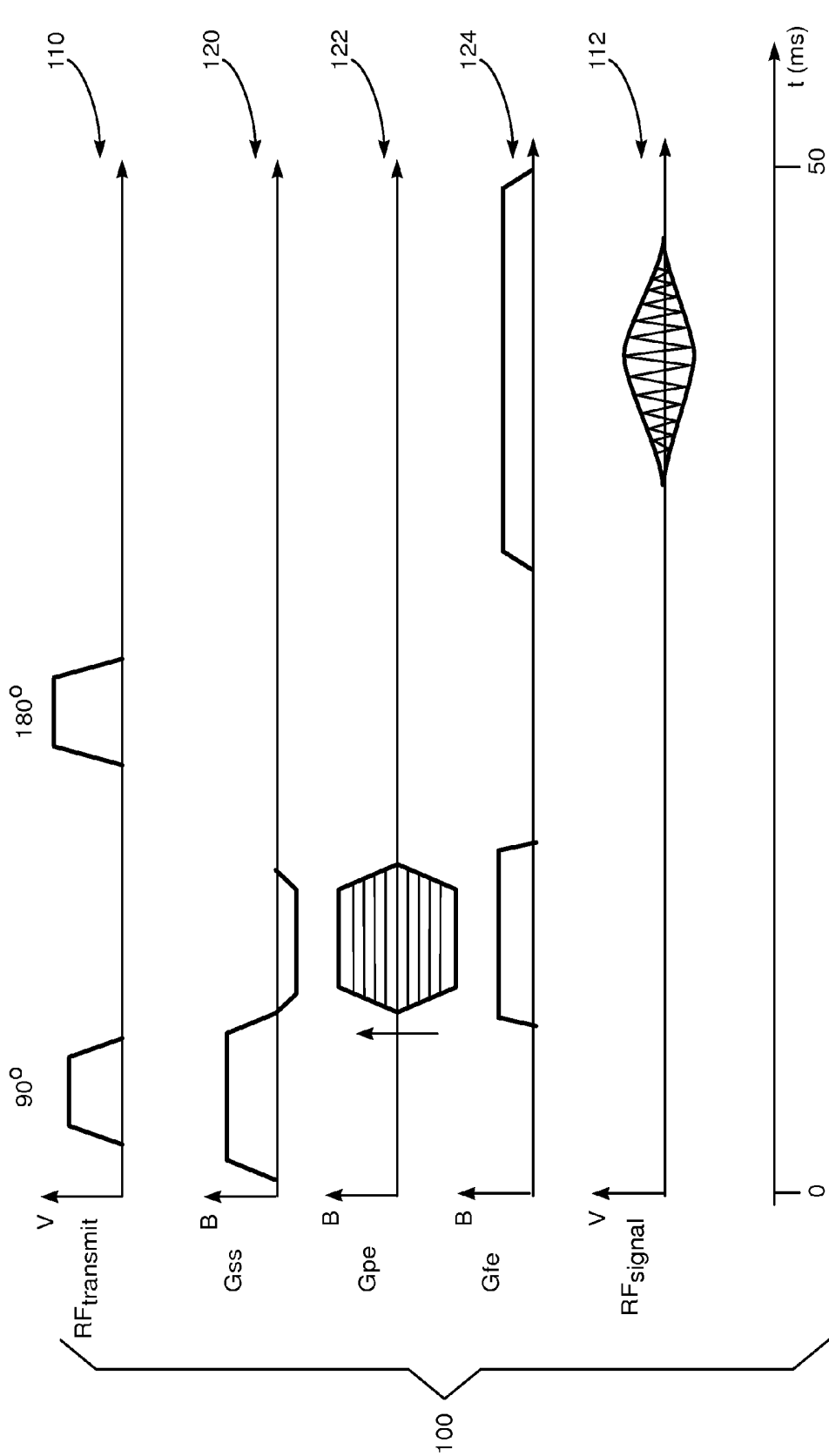


FIG. 3

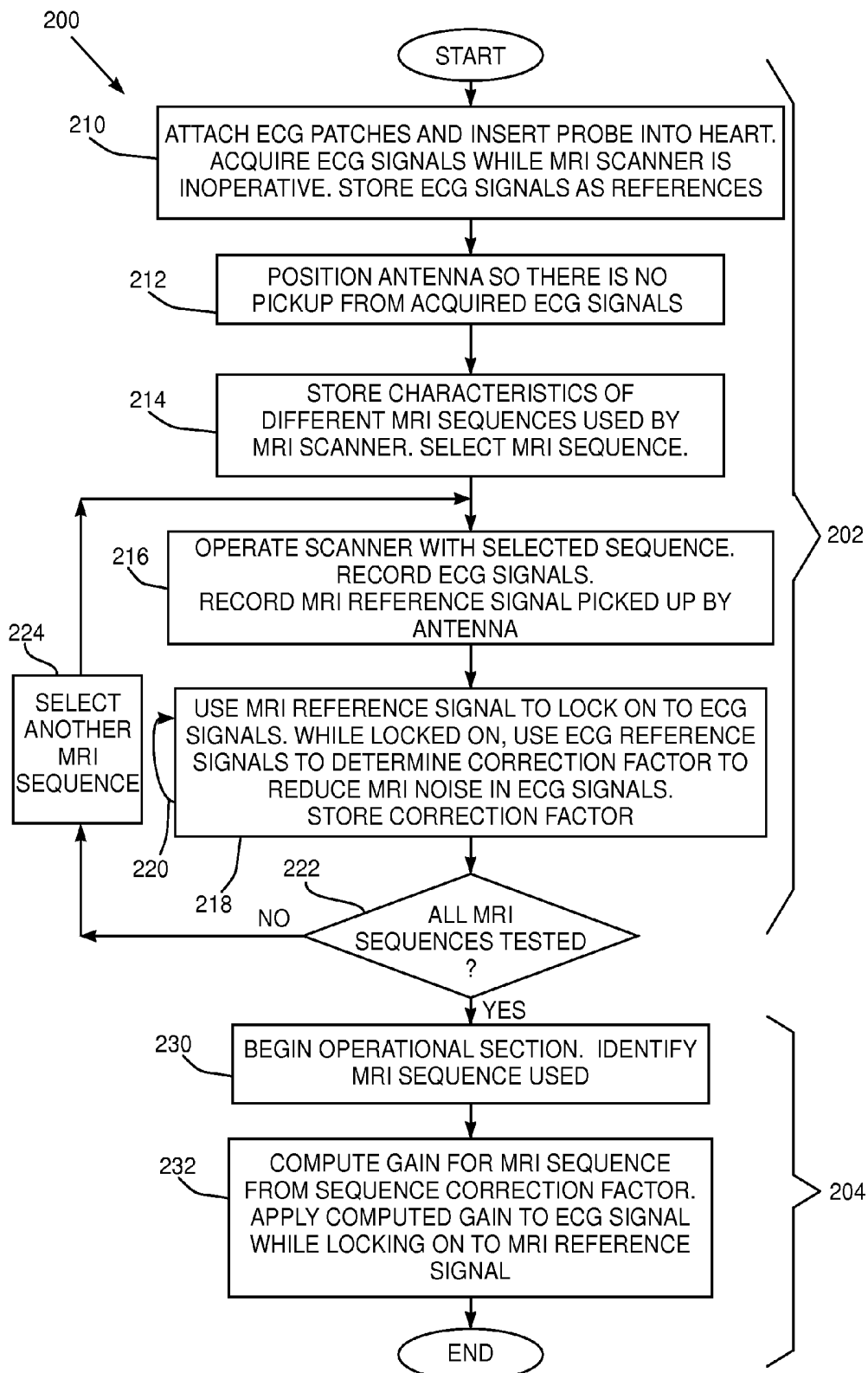


FIG. 4

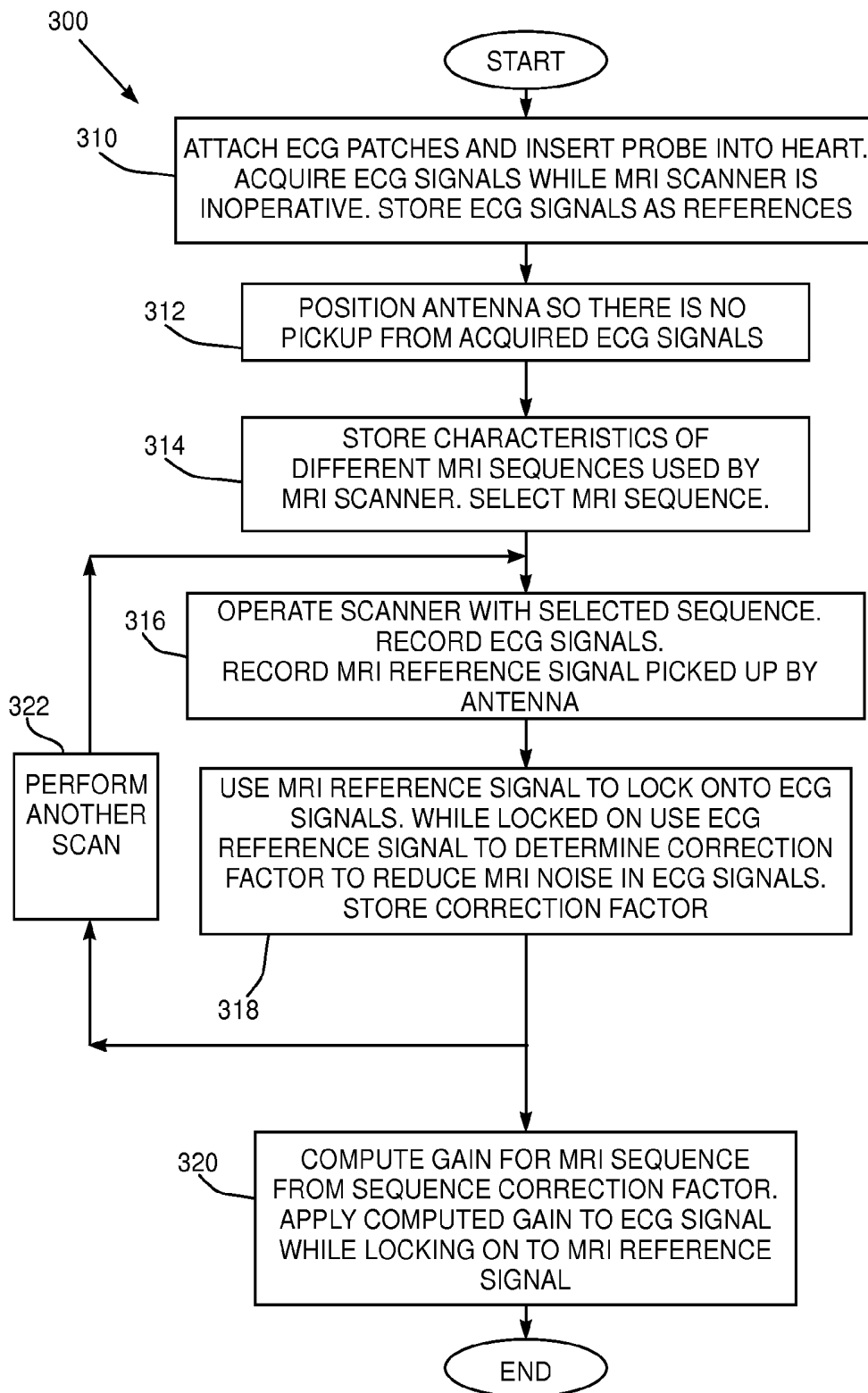


FIG. 5

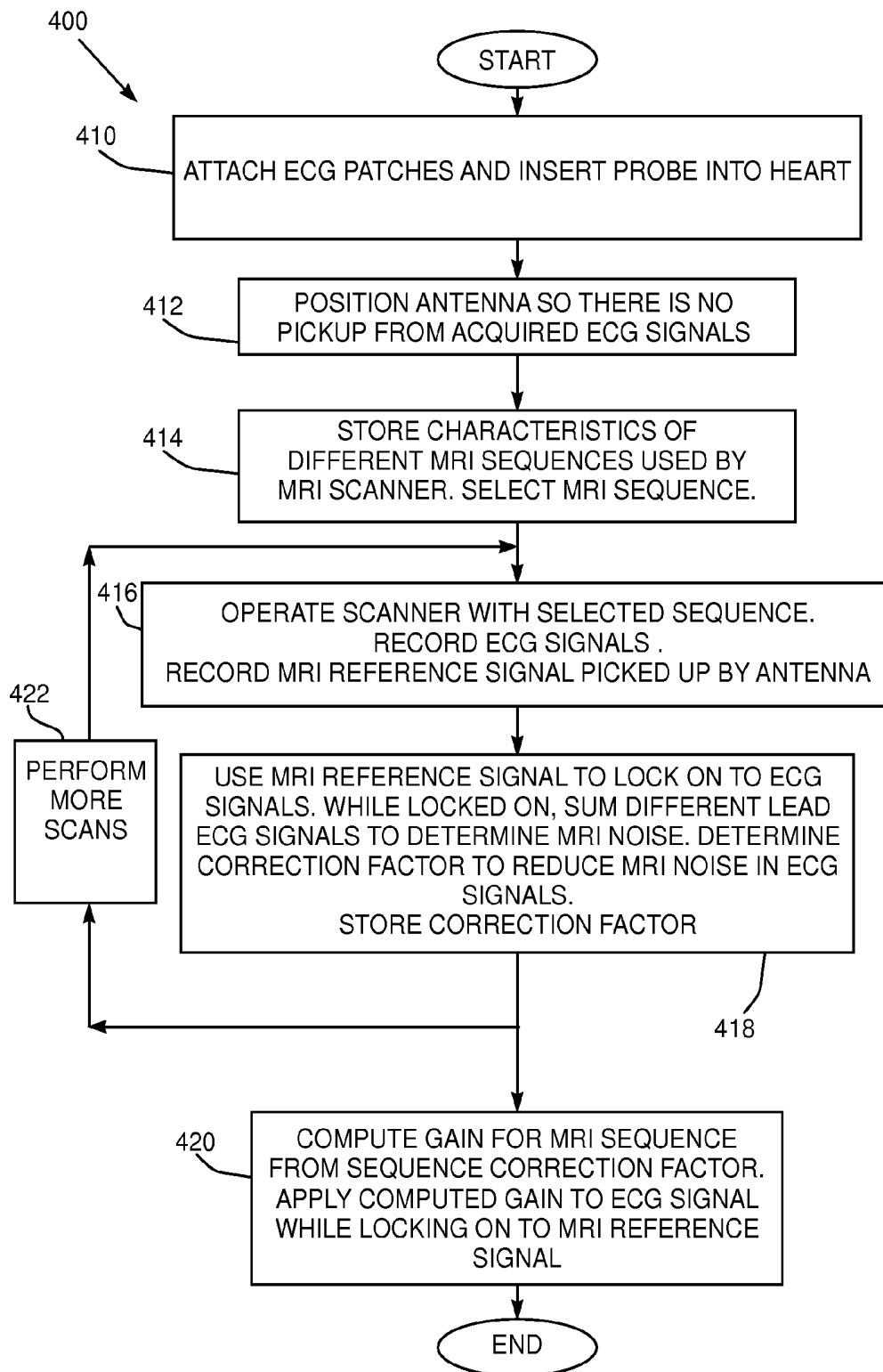


FIG. 6

**ANALOG CANCELLATION OF MRI  
SEQUENCING NOISE APPEARING IN AN  
ECG SIGNAL**

CROSS-REFERENCE TO RELATED  
APPLICATION

[0001] This application is related to U.S. patent application entitled "Dynamic Cancellation of MRI Sequencing Noise Appearing in an ECG Signal," filed on even date, which is assigned to the assignees of the present invention, and which is incorporated herein by reference.

FIELD OF THE INVENTION

[0002] The present invention relates generally to electrocardiograph (ECG) signals, and specifically to detecting the ECG signals during a magnetic resonance imaging (MRI) procedure.

BACKGROUND OF THE INVENTION

[0003] Magnetic resonance imaging (MRI) is an extremely powerful technique for visualizing tissue, particularly soft tissue, of a patient. The technique relies on exciting nuclei, typically hydrogen nuclei, from their equilibrium state, and measuring the resonant radio-frequency signals emitted by the nuclei as they relax back to equilibrium.

[0004] In an MRI procedure the cardiac condition of a patient placed in the rapidly changing magnetic fields generated by the procedure may need to be assessed. Monitoring of an electrocardiograph (ECG) signal is a good indicator of the cardiac condition of the patient, so that ECG monitoring may enhance the efficacy of the procedure.

[0005] U.S. Pat. No. 6,873,869, to Fischer, whose disclosure is incorporated herein by reference, describes a method of obtaining an ECG signal of a patient located in a turbulent electromagnetic environment. The signal, including added noise, is recovered near the cardiac region as a differential signal resulting from signals delivered by two electrodes forming part of a first measurement loop.

[0006] U.S. Pat. No. 5,217,010, to Tsitlik, et al., whose disclosure is incorporated herein by reference, describes a device for monitoring a patient or pacing a patient which is stated to be able to safely operate in an MRI system. The device claims to use unique RF filtering and shielding to attenuate voltages on the leads resulting from the high frequency RF signals produced in the MRI.

[0007] U.S. Patent Application 2004/0225210, to Brosovich, et al., whose disclosure is incorporated herein by reference, describes a lead set assembly which is stated to be capable of coupling electrodes to a separate device. The assembly includes two leads. A condition sense lead features two conductive paths, each being connectible to one electrode for conveying a bioelectric signal therefrom and which is capable of having a first noise signal induced therein by electromagnetic emanations. A noise pickup lead also features two conductive paths, each being capable of having a second noise signal induced therein by the electromagnetic emanations.

[0008] U.S. Pat. No. 7,039,455, to Brosovich, et al., whose disclosure is incorporated herein by reference, describes apparatus for improving the quality of ECG signals obtained from a patient undergoing MRI. The apparatus includes the

arrangement of a differential amplifier, a prefilter, a signal limiter circuit and an intermediate amplifier with an integral low pass filter.

[0009] U.S. Pat. No. 7,286,871, to Cohen, whose disclosure is incorporated herein by reference, describes a method of reducing contamination of electrical signals recorded in the presence of repeated interference contamination. The electrical signal is digitized, the digitizing beginning with a timing signal. A plurality of digitized electrical signals is analyzed, and the electrical signals are synchronized with respect to the timing signal, to obtain an estimated contaminating signal that is subtracted from the digitized electrical signal.

[0010] U.S. Pat. No. 4,991,580, to Moore, whose disclosure is incorporated herein by reference, describes a method for improving the quality of ECG signals obtained from a patient undergoing MRI. The method includes conducting the ECG signals having MRI induced noise signals to the input of a slew rate limiter (SRL) circuit having a preselected maximum slew rate. The output of the SRL circuit is connected to a low pass filter circuit.

[0011] U.S. Pat. No. 6,070,097, to Kreger, et al., whose disclosure is incorporated herein by reference, describes a method for generating a gating signal for cardiac MRI. An MRI system includes a detector system which receives an ECG signal from a patient being scanned and produces the gating signal. The gating signal is produced when a detected peak in the ECG signal meets a set of R-wave criteria.

[0012] European Patent 1,872,715, to Uutela Kimmo, whose disclosure is incorporated herein by reference, describes reference data indicative of statistical properties of biosignal artifacts that is generated by a turbulent electromagnetic environment and that is collected. Multiple channels of the biosignal of the patient are measured in the turbulent electromagnetic environment. Artifacts in the multiple channels are detected using the reference data and parameters are derived for a linear combination of the multiple channels. A refined biosignal is obtained by applying a linear combination to desired signal samples of the multiple channels, the linear combination being defined by the parameters derived.

[0013] PCT application WO/2012/170119, to Schweitzer et al., whose disclosure is incorporated herein by reference, describes a system for tracking catheter electrode locations with the body of a patient during an MRI scan sequence. The system includes mitigation logic configured to identify one or more impedance measurements that were taken during potentially noise-inducing conditions, and were thus subject to corruption by noise. The mitigation logic is configured to replace the potentially corrupt impedance measurements with previously-obtained impedance measurements taken from an immediately preceding acquisition cycle.

[0014] An article titled "Cardiac MRI: Part 2, Pericardial Diseases" by Prabhakar Rajiah, in Volume 197, Issue 4 of the American Journal of Roentgenology, published in October 2011, describes the use of MRI in cardiac procedures.

[0015] Documents incorporated by reference in the present patent application are to be considered an integral part of the application except that to the extent any terms are defined in these incorporated documents in a manner that conflicts with the definitions made explicitly or implicitly in the present specification, only the definitions in the present specification should be considered.

## SUMMARY OF THE INVENTION

**[0016]** An embodiment of the present invention provides a method, including:

**[0017]** while imaging a patient using an initial magnetic resonance imaging (MRI) sequence, generating an initial MRI reference signal in response to the initial MRI sequence using a reference sensor placed in proximity to the patient;

**[0018]** identifying, by locking on to the initial MRI reference signal, noise that will be generated in electrocardiograph (ECG) signals received from the patient;

**[0019]** computing a programmable correction to be applied to the ECG signals to reduce the noise; and

**[0020]** applying the programmable correction to reduce the noise in the ECG signals, received from the patient, while imaging the patient using a subsequent MRI sequence and while locking on to a subsequent MRI reference signal generated in response to the subsequent MRI sequence using the reference sensor.

**[0021]** Typically the method includes placing the reference sensor so as not to pick up the ECG signals.

**[0022]** In a disclosed embodiment the reference sensor consists of an antenna.

**[0023]** In a further disclosed embodiment the programmable correction includes a set of frequency dependent gains.

**[0024]** In a yet further disclosed embodiment identifying the noise consists of analyzing the ECG signals generated from stationary electrodes coupled to the patient.

**[0025]** In an alternative embodiment identifying the noise includes comparing the ECG signals received from the patient while not imaging the patient with an MRI sequence to the ECG signals received from the patient while imaging the patient using the initial MRI sequence.

**[0026]** In a further alternative embodiment identifying the noise includes summing the ECG signals received from the patient while imaging the patient using the initial MRI sequence. Typically, summing the ECG signals consists of summing the ECG signals generated from stationary electrodes coupled to the patient.

**[0027]** There is further provided, according to an embodiment of the present invention, apparatus, including:

**[0028]** a reference sensor, placed in proximity to a patient, and configured, while the patient is imaged using an initial magnetic resonance imaging (MRI) sequence, to generate an initial MRI reference signal in response to the initial MRI sequence; and

**[0029]** a processor, which is configured:

**[0030]** to identify, by locking on to the initial MRI reference signal, noise that will be generated in electrocardiograph (ECG) signals received from the patient,

**[0031]** to compute a programmable correction to be applied to the ECG signals to reduce the noise, and

**[0032]** to apply the programmable correction to reduce the noise in the ECG signals, received from the patient, while imaging the patient using a subsequent MRI sequence and while locking on to a subsequent MRI reference signal generated in response to the subsequent MRI sequence using the reference sensor.

**[0033]** The present invention will be more fully understood from the following detailed description of the embodiments thereof, taken together with the drawings in which:

## BRIEF DESCRIPTION OF THE DRAWINGS

**[0034]** FIG. 1 is a schematic, pictorial illustration of a system for analog cancellation of magnetic resonance imaging (MRI) noise appearing in electrocardiograph (ECG) signals, according to an embodiment of the present invention;

**[0035]** FIG. 2 is a set of voltage vs. time and magnetic field vs. time graphs schematically illustrating a sequence of MRI signals generated during an MRI procedure, according to an embodiment of the present invention;

**[0036]** FIG. 3 is an alternative set of voltage vs. time and magnetic field vs. time graphs schematically illustrating a sequence of MRI signals generated during an MRI procedure, according to an embodiment of the present invention;

**[0037]** FIG. 4 is a flowchart of steps performed in implementing the system of FIG. 1, according to an embodiment of the present invention;

**[0038]** FIG. 5 is a flowchart of steps performed in implementing the system of FIG. 1, according to an alternative embodiment of the present invention; and

**[0039]** FIG. 6 is a flowchart of steps performed in implementing the system of FIG. 1, according to a further alternative embodiment of the present invention.

## DETAILED DESCRIPTION OF EMBODIMENTS

## Overview

**[0040]** An embodiment of the present invention reduces magnetic resonance imaging (MRI) noise that is picked up in electrocardiograph (ECG) signals received from a patient, while the patient is imaged by an MRI sequence. In order to reduce the noise a sensor, typically an antenna, that is able to detect MRI radiation from an MRI scanner, is positioned in proximity to the patient. The sensor is typically positioned so that it does not pick up ECG signals from the patient, but so that it produces a signal, used as an MRI reference signal, that supports a processor in reducing the MRI noise.

**[0041]** In some embodiments the noise is first detected and characterized using a training phase. The training phase is followed by an operational phase, wherein a correction factor generated in the training phase is applied

**[0042]** In the training phase, ECG signals from the patient are first recorded while the MRI sequence is not operative. These signals are used as ECG reference signals. The MRI sequence is then activated, so generating the MRI reference signal described above, as well as introducing MRI noise into the ECG signals. The processor uses the MRI reference signal to lock onto the ECG signals, and compares the reference ECG signals with those generated while being locked on. Using the comparison, the processor generates a correction factor, typically a set of frequency dependent gains which may be applied to the ECG signals so as to reduce the MRI noise.

**[0043]** Respective correction factors may be generated for different types of MRI sequence, as well as for variations of defining parameters of each type of sequence.

**[0044]** In the operational phase, a correction factor is applied to subsequent ECG signals generated during subsequent MRI sequences, while locking on to the MRI reference signal generated during activation of the sequence. Typically the type of sequence, as well as the parameters defining the sequence, may be identified from the MRI reference signal.

**[0045]** In alternative embodiments of the present invention, there is no training phase. Rather, the introduced MRI noise is

detected, and reduced, during the operational phase, using methods similar to those described above. The detection and reduction may be performed in an “on-the-fly” manner, using iteration to improve the detection and reduction of the injected MRI noise.

#### DETAILED DESCRIPTION

**[0046]** Reference is now made to FIG. 1, which is a schematic, pictorial illustration of a system 20 for analog cancellation of magnetic resonance imaging (MRI) sequencing noise appearing in electrocardiograph (ECG) signals, according to an embodiment of the present invention. System 20 comprises an MRI scanner 22, a probe 24, such as a catheter, and a control console 26. Probe 24 may be used for acquiring ECG signals in a chamber of a heart 28 of a patient 30, using one or more electrodes 32 in a distal end 34 of the probe. Signals acquired by electrodes 32 are herein termed internal ECG signals. In some embodiments, probe 24 may be used for additional purposes, such as for performing cardiac ablation. Further alternatively, probe 24 may be used, mutatis mutandis, for other therapeutic and/or diagnostic functions in the heart or in other body organs. The internal ECG signals acquired by electrodes 32 are transferred, typically by conductors and/or optical fibers in probe 24, to control console 26, wherein the signals may be analyzed.

**[0047]** In addition to acquiring internal ECG signals using probe 24, system 20 typically also acquires ECG signals from the skin of patient 30, typically by placing a number of conductive patches 36, which act as electrodes, on the skin of the patient. Signals acquired by patches 36 are herein termed external ECG signals. External ECG signals are conveyed via a cable 38 to control console 26, which analyzes the signals. Results derived from the analysis may be presented on a display 40 to an operator 42 of system 20.

**[0048]** Operator 42, typically a cardiologist, inserts probe through the vascular system of patient 30 so that distal end 34 of the probe enters a body cavity, herein assumed to be the cardiac chamber from where the internal ECG signals are acquired. Typically the distal end of the probe is tracked by a method known in the art. Magnetic position tracking techniques are described, for example, in U.S. Pat. Nos. 5,391,199, 5,443,489, 6,788,967, 6,690,963, 5,558,091, 6,172,499, 6,177,792, whose disclosures are incorporated herein by reference. Impedance-based position tracking techniques are described, for example, in U.S. Pat. Nos. 5,983,126, 6,456,864 and 5,944,022, whose disclosures are also incorporated herein by reference.

**[0049]** MRI scanner 22 comprises magnetic field coils 50, including field gradient coils, which together generate a spatially variant magnetic field  $B(x,y,z)$ . The spatially variant magnetic field provides spatial localization for radio frequency (RF) signals generated in the scanner. In addition, the scanner comprises transmit/receive coils 52. In a transmit mode coils 52 radiate RF pulsed energy to patient 30, the RF pulses of energy interacting with the nuclear spins of the patient's tissue and thereby realigning the magnetic moments of the nuclei away from their equilibrium positions. In a receive mode, coils 52 detect RF signals received from the patient's tissue as the tissue nuclei relax to their equilibrium state. The frequency of the signals generated by the relaxation of nuclei in a given region, the Larmor frequency, is directly proportional to the magnetic field at the region, with a constant of proportionality given by the gyromagnetic ratio  $\gamma$  of the nuclei. Thus, for hydrogen nuclei, equation (1) applies:

$$f(x, y, z) = \frac{\gamma}{2\pi} \cdot B(x, y, z) \quad (1)$$

**[0050]** where  $f(x,y,z)$  is the frequency radiated by the relaxing hydrogen nuclei from a point  $(x,y,z)$ ,

**[0051]**  $B(x,y,z)$  is the magnetic field at the point, and

$$\frac{\gamma}{2\pi}$$

is equal to approximately  $42.6 \text{ MHz} \cdot \text{T}^{-1}$ .

**[0052]** System 20 also comprises an MRI reference sensor 54, typically an antenna, and which may also be referred to herein as antenna 54. Antenna 54 generates a signal in response to operation of scanner 22, by picking up MRI radiation from coils 50 and 52. Antenna 54 is connected by a cable 55, typically a coaxial cable, to console 26. As is described later on, system 20 uses the antenna signal, typically after it has been transferred through an isolating differential amplifier (not shown) as an MRI reference signal. While sensor 54 is typically an antenna, the scope of the present invention includes any type of sensor, such as a semiconductor sensor, that is able to generate a signal by picking up MRI radiation.

**[0053]** In some embodiments, scanner 22 is operated by a scanner processor 56, and the ECG and MRI reference signals described above are analyzed by an ECG processor 58. Processor 58 typically also tracks the probe acquiring the internal ECG signals. For simplicity, in the description herein a single processor 60 in console 26 is assumed to operate system 20, and those having ordinary skill in the art will be able to adapt the description in the event that more than one processor operates the system.

**[0054]** Thus, in addition to analyzing the ECG and MRI reference signals referred to above, and tracking the probe acquiring the internal ECG signals, processor 60 operates scanner 22 by using circuitry to control coils 50, including forming required magnetic field gradients, as well as other circuitry to operate transmit/receive coils 52.

**[0055]** Processor 60 typically comprises a general-purpose computer, which is programmed in software to carry out the functions that are described herein. The software may be downloaded to processor 60 in electronic form, over a network, for example, or it may be provided on non-transitory tangible media, such as optical, magnetic or electronic memory media. Alternatively, some or all of the functions of processor 60 may be carried out by dedicated or programmable digital hardware components, or by using a combination of hardware and software elements.

**[0056]** FIG. 2 is a first set of voltage (V) vs. time (t) and magnetic field (B) vs. time (t) graphs schematically illustrating a sequence 70 of MRI signals generated during an MRI procedure, according to an embodiment of the present invention. A first voltage vs. time graph 72 illustrates a transmit RF pulse 74, generated by coils 52, which is transmitted at the start of sequence 70. The transmit RF pulse length is typically of the order of 2 ms, although it may be larger or smaller than this. Encompassing the transmit RF pulse, illustrated in a first magnetic field vs. time graph 76, is a slice selection gradient (G<sub>ss</sub>) magnetic field pulse generated by coils 50. The slice selection gradient field identifies a volume of interest in patient 30 that is to be imaged by scanner 22.

**[0057]** A second magnetic field vs. time graph **80** illustrates a phase encoding gradient (Gpe) field pulse, which selects a vertical position of points within the volume of interest. A third magnetic field vs. time graph **84** illustrates a frequency encoding gradient (Gfe) field pulse, which selects a horizontal position of points within the volume of interest.

**[0058]** A second voltage vs. time graph **88** illustrates a receive RF pulse **90**, corresponding to the data acquisition signal received by coils **52** in response to the transmit RF pulse.

**[0059]** A typical time between the center of the RF transmit pulse and the center of the RF receive pulse may be approximately 30 ms. A typical time for the overall sequence may be approximately 40 ms. However, the actual times may be larger or smaller than these values.

**[0060]** During the course of an MRI procedure, the sequence of RF pulses and magnetic field settings, illustrated by sequence **70**, may be repeated, typically at a repetition rate of the order of 1 s. At each repetition of sequence **70**, one or more of the variables defining the magnetic field pulses may be varied, typically so that different regions of patient **36** may be scanned. In some cases, as sequence **70** is repeated, variables of RF transmit pulse **74**, such as its amplitude, frequency, or phase, may be changed.

**[0061]** Sequence **70** illustrates one type of MRI sequence, termed a gradient echo sequence, that is typically used in an MRI procedure.

**[0062]** FIG. **3** is a second set of voltage vs. time and magnetic field vs. time graphs schematically illustrating a sequence **100** of MRI signals generated during an MRI procedure, according to an embodiment of the present invention. As for sequence **70**, sequence **100** comprises transmit and receive voltage vs. time graphs **110** and **112**, and three magnetic field vs. time graphs **120**, **122**, and **124**. As is illustrated in the graphs, sequence **100** uses two RF transmit pulses and two magnetic field Gfe pulses (in contrast to the one RF pulse and one Gfe pulse of sequence **70**). Sequence **100** illustrates a spin echo sequence, that may typically also be used in an MRI procedure.

**[0063]** FIGS. **2** and **3** illustrate two types of MRI sequence that may be used in embodiments of the present invention. Variations on these sequences, as well as other possible sequences, will be apparent to those having ordinary skill in the art, and all such sequences are assumed to be within the scope of the present invention. In the following description, an identifier "m" is used to label each type of MRI sequence, and by way of example the MRI sequence illustrated by FIG. **2** is assumed to have identifier m=1, and the MRI sequence illustrated by FIG. **3** is assumed to have identifier m=2.

**[0064]** FIGS. **2** and **3** also illustrate that each MRI sequence is comprised of a number of phases, corresponding to the different pulses that are generated for the sequence. A phase of an MRI sequence may be defined in terms of a pulse, a number of pulses, and/or parts of a pulse. For example, a selected phase of the MRI sequence of FIG. **2** may be defined as the duration of the Gpe pulse; for the MRI sequence of FIG. **3**, another selected phase may be defined as the duration of a first half of the second Gfe pulse.

**[0065]** In general, any MRI sequence may be defined in terms of the variables describing each of the pulses graphed in FIGS. **2** and **3**. Thus, referring to voltage vs. time graphs **72** and **110**, the variables comprise the frequency, phase, and amplitude of the voltage of the RF pulse initiating a sequence, changes in values of these variables over time, variables of

any subsequent RF pulses, and timing of the subsequent RF pulses with respect to the initial RF pulse. Referring to magnetic field vs. time graphs **76**, **80**, and **84**, and graphs **120**, **122**, and **124**, the variables include those describing the shape of the magnetic field pulses, i.e., the amplitude of the field as it varies in time, and timing of the magnetic field pulses with respect to the RF pulse or pulses in graphs **72** and **112**, and with respect to each other.

**[0066]** More specifically, each MRI sequence m may be characterized broadly in terms of a set of parameters, each parameter corresponding to one of the pulses of the sequence. In the following description, the set of parameters for an MRI sequence m is written as  $\{S\}_m$ .

**[0067]** For example, MRI sequence m=1, illustrated in FIG. **2**, may have a set of parameters  $\{S\}_1 = \{P_{RF}, P_{Gss}, P_{Gpe}, P_{Gfe}, P_{signal}\}$ , each of the elements of the set representing a voltage or a magnetic field pulse. In contrast, MRI sequence m=2, illustrated in FIG. **3**, has a set of parameters  $\{S\}_2 = \{P_{RF1}, P_{RF2}, P_{Gss}, P_{Gpe}, P_{Gfe1}, P_{Gfe2}, P_{signal}\}$ .

**[0068]** For any given MRI sequence m, there is a further, more detailed, characterization of each of the parameters in the set. Thus, referring to voltage vs. time graph **72** of m=1, parameter  $P_{RF}$  is characterized in terms of the variables frequency f, phase  $\phi$ , and amplitude A of the voltage of the RF pulse initiating a sequence, and changes in values of these variables over time t.  $P_{RF}$  may thus be represented as a set of ordered 4-tuples, which may be written as an equation (2):

$$P_{RF} = \{(f, \phi, A, t)\}_1 \quad (2)$$

**[0069]** where the set subscript is the identifier m of the sequence.

**[0070]** Similarly, referring to magnetic field Gss vs. time graph **76** of m=1, parameter  $P_{Gss}$  is characterized in terms of the variable magnetic field B at time t, so that  $P_{Gss}$  may be represented as a set of ordered pairs of variables, which may be written as an equation (3):

$$P_{Gss} = \{(B, t)\}_1 \quad (3)$$

**[0071]** Referring to voltage vs. time graph **110** of m=2, parameters  $P_{RF1}$  and  $P_{RF2}$  may be represented by the equations:

$$P_{RF1} = \{(f_1, \phi_1, A_1, t)\}_2 \quad (4)$$

and

$$P_{RF2} = \{(f_2, \phi_2, A_2, t)\}_2 \quad (5)$$

**[0072]** where  $f_1, \phi_1, A_1$  are the frequency, phase and amplitude variables at time t of the first pulse of m=2, and

**[0073]**  $f_2, \phi_2, A_2$  are the frequency, phase and amplitude variables at time t of the second pulse of m=2.

**[0074]** As another example, referring to field vs. time graph **124**, parameters  $P_{Gfe1}, P_{Gfe2}$  may be represented by the equations:

$$P_{Gfe1} = \{(B_1, t)\}_2 \quad (6)$$

and

$$P_{Gfe2} = \{(B_2, t)\}_2 \quad (7)$$

**[0075]** where  $B_1$  and  $B_2$  are the field variables of the first Gfe pulse and the second Gfe pulse at time t.

**[0076]** Prior to operating scanner **22**, operator **42** uses processor **60** to store  $\{S\}_m$ , in terms of its parameters and the variables associated with each parameter (in the broad and more detailed manner described above) for each MRI

sequence  $m$ . During a procedure where scanner **22** is operated, the processor recalls the parameters and variables of  $\{S\}_m$  as is explained below with reference to the flowchart of FIG. 4. A specific set of numerical values defining the values of the parameters and variables of  $\{S\}_m$  is referred to hereinbelow as  $\{S\}_{mp}$ , where  $p$  is an index representing the numerical values.

[0077] FIG. 4 is a flowchart **200** of steps performed in implementing system **20**, according to an embodiment of the present invention. The flowchart is divided into two sections: a training phase or section **202** and an operational phase or section **204**. The description of the flowchart assumes that appropriate steps of the flowchart are implemented using single processor **60**. If system **20** comprises scanner processor **56** and ECG processor **58**, then the flowchart steps may be assumed to be implemented by ECG processor **58**, using communications as to the timing and identity of MRI sequence  $m$ , and as to the numerical values  $p$  of the sequence, from scanner processor **56**.

[0078] In an initial step **210** of the training phase, operator **42** attaches patches **36** to patient **30**, and inserts probe **24** into heart **28** of the patient. Patches **36** acquire external ECG signals, and the electrode or electrodes of probe **24** acquire internal ECG signals, while scanner **22** is inoperative. Processor **60** receives the acquired ECG signals, and stores a selected group of the signals as a reference set of signals.

[0079] Typically, the reference set of signals comprises signals from electrodes which are relatively stationary with respect to patient **30**. For example, the reference set of signals may be from patches **36**. In some embodiments probe **24** may be stationary, e.g., if it is being used as an internal reference probe in heart **28**, in which case other movable probes (not shown in FIG. 1) may be inserted into heart **28**. If probe **24** is stationary, then signals from its electrode or electrodes may be used as ECG reference signals. In some embodiments the reference set may comprise a sub-set of patch signals, such as a selected one of the signals from the patches, and/or a sub-set of signals from electrodes of probe **24** if the probe is stationary.

[0080] In an antenna setup step **212**, antenna **54** is positioned in proximity to patient **30**, typically above a covering of the patient. The location and orientation of the antenna are chosen so that there is no pickup by the antenna of ECG signals generated by the patient. For example, the antenna may be positioned above the patient's abdominal area.

[0081] In a characterization step **214**, the processor stores the parameters and the variables of the different MRI sequences to be used in operating system **20**. In other words, the processor stores the sets  $\{S\}_m$  for each value of  $m$  to be used in the procedure. Once the parameters and the variables have been stored the processor selects an MRI sequence  $m$  with which to operate the scanner, and a set  $\{S\}_{mp}$  of numerical values for the sequence.

[0082] In a recording step **216**, scanner **22** is operated using the selected MRI sequence, and the processor acquires and records ECG signals, from patches **36** and from the electrodes of probe **24**, generated while the scanner operates. The recorded ECG signals are selected to correspond with, i.e., to be on the same leads as, the reference signals stored in step **210**. The recorded ECG signals include noise, injected, inter alia, into the leads conveying the signals, because of the scanner operation. The scanner operation is typically for a

multiplicity of scans of the sequence, although there is no requirement for this, and the operation may be for single scan of the sequence.

[0083] In addition, while acquiring and recording the ECG signals, and while scanner **22** is being operated, in step **216** the processor also acquires and records the signal generated in sensor **54**, the MRI reference signal.

[0084] In a correction determining step **218**, the recorded ECG signals of step **216** are compared with the reference set of ECG signals stored in step **210**, while locking onto the MRI reference signal. From the comparison, the processor determines a correction factor to be applied to the recorded ECG signals so that the resultant ECG signals approximate to the reference signals. The correction factor is typically a set of gains  $\{G\}$  which are frequency dependent, and which are applied by the processor to the recorded ECG signals, although in some embodiments the correction factor may be a single value gain. There is a set of gain values for each MRI sequence  $m$ , and for the set of numerical values  $\{S\}_{mp}$  associated with the  $m$  sequence.

[0085] Using tested  $p$  values processor generates, typically by interpolation and/or extrapolation, an expression,  $\{G\}_{mp}$ , for the correction factor to be applied for any sequence  $m$  and for any numerical value  $p$  within the sequence, as given by equation (8).

$$\{G\}_{mp} = \{(G_{if})_{mp}\} \quad (8)$$

[0086] where  $G_i$  is the gain applied at frequency  $f_i$ , and where  $i$  is an identifier of the frequency.

[0087] It will be understood that  $\{G\}_{mp}$  represents the set of gains and associated frequencies required to reduce the noise generated by MRI sequence  $m$  for the sequence numerical values having an index  $p$ .

[0088] Typically, as shown by an arrow **220**, for a given value of  $m$  step **218** is repeated a number of times, for different values of  $p$ , so that the values of the specific gains  $G_i$  and frequencies  $f_i$  in equation (8) may be determined more exactly. The repetition also allows for a range of  $p$  values.

[0089] In a decision step **222**, the processor checks if all MRI sequences have been tested, i.e., if gains for all values of  $m$  in equation (8) have been generated. If a sequence remains, the flowchart proceeds to step **224** to select another MRI sequence, and then returns to step **216**. If all sequences have been analyzed, training section **202** concludes and operational section **204** begins.

[0090] In a first step **230** of the operational section, the processor identifies the MRI sequence  $m$  being used. The processor also determines the specific numerical values of  $\{S\}_{mp}$  being used for the sequence. The identification of  $m$  and  $\{S\}_{mp}$  may be made by communication from scanner **22**. Alternatively or additionally, the processor may analyze characteristics of the MRI reference signal picked up by sensor **54** in order to identify  $m$  and the associated numerical values.

[0091] In a final step **232** of the operational section, the processor computes the correction factor, i.e., the gains to be applied, from equation (8). The processor then applies the calculated gains to all the ECG signals received from patches **36** and from the electrodes of probe **24**, while the MRI sequence is operative, so as to reduce the MRI noise in the signals. The processor determines operation of the MRI sequence by locking on to the MRI reference signal generated in sensor **54**.

[0092] The description above of flowchart **200** assumes that a complete MRI sequence  $m$  is being considered, and that

gains given by equation (8) are applied to the ECG signals acquired while the complete sequence is operative. Those having ordinary skill in the art will be able to adapt the description, mutatis mutandis, for the case that noise from one or more phases of MRI sequence *m* is created in the ECG signals, and that the noise for each phase is to be reduced separately. In this case equation (8) may be used to calculate gains to be applied during each separate phase, and the separate phases may be identified, in both the training and operational sections of the flowchart, from the MRI reference signal generated in sensor **54**, and/or by communications from scanner **22**.

[0093] The description of flowchart **200** has also assumed that system **20** is implemented using training section **202** followed by operational section **204**. However, in alternative embodiments of the present invention there is no requirement for a separate training section, and in these embodiments the training of system **20** is performed “on-the-fly.” The steps of flowcharts **300** and **400**, described below with reference to FIGS. **5** and **6**, exemplify how system **20** may be implemented during performance of an MRI procedure on a patient, without a separate training section.

[0094] FIG. **5** is a flowchart **300** of steps performed in implementing system **20**, according to an alternative embodiment of the present invention. First, second, and third steps **310**, **312**, and **314** are substantially as described for steps **210**, **212**, and **214** of flowchart **200**, respectively storing reference ECG signals typically derived from stationary electrodes, positioning antenna **54**, and storing MRI sequence characteristics. A recording step **316** is generally the same as step **216**. However, typically the ECG recording is for a small number of MRI scans, or for a single scan.

[0095] A correction determining step **318** is also generally the same as step **218**. Thus, the processor determines a correction factor, typically in terms of gains given by equation (8), that are to be applied to the recorded ECG signals so that the resultant ECG signals approximate to the ECG reference signals.

[0096] The flowchart then proceeds to a final step **320**.

[0097] Typically, as indicated by an iteration step **322**, where the scanner is operated for another scan, steps **316** and **318** are iterated. As the iteration continues, the processor is able to improve the accuracy of the gains derived from equation (8) and generated in step **318**.

[0098] Final step **320** is substantially the same as final step **232**, the processor applying the gains derived in step **318** to all the ECG signals, while locking on to the MRI reference signal.

[0099] FIG. **6** is a flowchart **400** of steps performed in implementing system **20**, according to a further alternative embodiment of the present invention. First, second, and third steps **410**, **412**, and **414** are generally the same as steps **210**, **212** and **214**, except that in step **410** there is no requirement to acquire ECG signals while the scanner is inoperative, and there is no storage of reference ECG signals.

[0100] A recording step **416** is substantially the same as step **216**. Typically, the recorded ECG signals are those from patches **36** and/or stationary electrodes of probe **24**. As for step **216**, in step **416** the processor also acquires and records the signal generated in sensor **54**, the MRI reference signal.

[0101] In a correction determining step **418** the processor, while locking on to the MRI reference signal, sums the recorded ECG signals from the patches or stationary electrodes. The summed signal provides the processor with an

estimate of the noise generated by operation of the MRI sequence. The processor uses the noise estimate to generate a correction factor, i.e., a set of gains represented by equation (8), to be applied to the ECG signals, so as to reduce the MRI noise in the signals.

[0102] The flowchart then proceeds to a final step **420**.

[0103] Typically, as indicated by an iteration step **422**, where the scanner is operated for another scan, steps **416** and **418** are iterated. As the iteration continues, the processor is able to improve the accuracy of the gains derived from equation (8) and generated in step **418**.

[0104] Final step **420** is substantially the same as final step **232**, the processor applying the gains derived in step **418** to all the ECG signals, while locking on to the MRI reference signal.

[0105] In the case that two separate processors **56** and **58** are operative, and that ECG processor **58** is used to implement the steps of flowcharts **200**, **300**, or **400**, scanner processor **56** may inform ECG processor **58** of appropriate entities associated with any given MRI sequence, such as the identity of the sequence, start and/or end times of the sequence, and start and/or end times of phases of the sequence.

[0106] Flowcharts **300** and **400** describe two different methods for operating system **20** without having a training section first. It will be appreciated that the methods described for the two flowcharts, for estimating the noise introduced into the ECG signals by the MRI scans, may be combined. Such a combination may lead to faster and/or more exact identification of the induced MRI noise, compared to applying the process of just one of the flowcharts.

[0107] It will thus be appreciated that the embodiments described above are cited by way of example, and that the present invention is not limited to what has been particularly shown and described hereinabove. Rather, the scope of the present invention includes both combinations and subcombinations of the various features described hereinabove, as well as variations and modifications thereof which would occur to persons skilled in the art upon reading the foregoing description and which are not disclosed in the prior art.

We claim:

1. A method, comprising:

while imaging a patient using an initial magnetic resonance imaging (MRI) sequence, generating an initial MRI reference signal in response to the initial MRI sequence using a reference sensor placed in proximity to the patient;

identifying, by locking on to the initial MRI reference signal, noise that will be generated in electrocardiograph (ECG) signals received from the patient;

computing a programmable correction to be applied to the ECG signals to reduce the noise; and

applying the programmable correction to reduce the noise in the ECG signals, received from the patient, while imaging the patient using a subsequent MRI sequence and while locking on to a subsequent MRI reference signal generated in response to the subsequent MRI sequence using the reference sensor.

2. The method according to claim 1, and comprising placing the reference sensor so as not to pick up the ECG signals.

3. The method according to claim 1, wherein the reference sensor comprises an antenna.

4. The method according to claim 1, wherein the programmable correction comprises a set of frequency dependent gains.

5. The method according to claim 1, wherein identifying the noise comprises analyzing the ECG signals generated from stationary electrodes coupled to the patient.

6. The method according to claim 1, wherein identifying the noise comprises comparing the ECG signals received from the patient while not imaging the patient with an MRI sequence to the ECG signals received from the patient while imaging the patient using the initial MRI sequence.

7. The method according to claim 1, wherein identifying the noise comprises summing the ECG signals received from the patient while imaging the patient using the initial MRI sequence.

8. The method according to claim 7, wherein summing the ECG signals comprises summing the ECG signals generated from stationary electrodes coupled to the patient.

9. Apparatus, comprising:

a reference sensor, placed in proximity to a patient, and configured, while the patient is imaged using an initial magnetic resonance imaging (MRI) sequence, to generate an initial MRI reference signal in response to the initial MRI sequence; and

a processor, which is configured:

to identify, by locking on to the initial MRI reference signal, noise that will be generated in electrocardiograph (ECG) signals received from the patient,

to compute a programmable correction to be applied to the ECG signals to reduce the noise, and

to apply the programmable correction to reduce the noise in the ECG signals, received from the patient, while

imaging the patient using a subsequent MRI sequence and while locking on to a subsequent MRI reference signal generated in response to the subsequent MRI sequence using the reference sensor.

10. The apparatus according to claim 9, wherein the reference sensor is placed so as not to pick up the ECG signals.

11. The apparatus according to claim 9, wherein the reference sensor comprises an antenna.

12. The apparatus according to claim 9, wherein the programmable correction comprises a set of frequency dependent gains.

13. The apparatus according to claim 9, and comprising stationary electrodes coupled to the patient, and wherein identifying the noise comprises analyzing the ECG signals generated from the stationary electrodes.

14. The apparatus according to claim 9, wherein identifying the noise comprises comparing the ECG signals received from the patient while not imaging the patient with an MRI sequence to the ECG signals received from the patient while imaging the patient using the initial MRI sequence.

15. The apparatus according to claim 9, wherein identifying the noise comprises summing the ECG signals received from the patient while imaging the patient using the initial MRI sequence.

16. The apparatus according to claim 15, and comprising stationary electrodes coupled to the patient, and wherein summing the ECG signals comprises summing the ECG signals generated from the stationary electrodes.

\* \* \* \* \*

专利名称(译)	模拟消除ECG信号中出现的MRI测序噪声		
公开(公告)号	<a href="#">US20150223712A1</a>	公开(公告)日	2015-08-13
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[标]申请(专利权)人(译)	韦伯斯特生物官能(以色列)有限公司		
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摘要(译)

一种方法，包括在使用初始磁共振成像（MRI）序列对患者成像的同时，使用放置在患者附近的参考传感器响应于初始MRI序列产生初始MRI参考信号。该方法还包括通过锁定初始MRI参考信号来识别将在从患者接收的心电图（ECG）信号中生成的噪声，并计算要应用于ECG信号的可编程校正以降低噪声。该方法还包括应用可编程校正以减少从患者接收的ECG信号中的噪声，同时使用随后的MRI序列对患者成像并且同时锁定响应于随后的MRI序列而产生的后续MRI参考信号。参考传感器。

