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(54) **DEVICE IDENTIFICATION**

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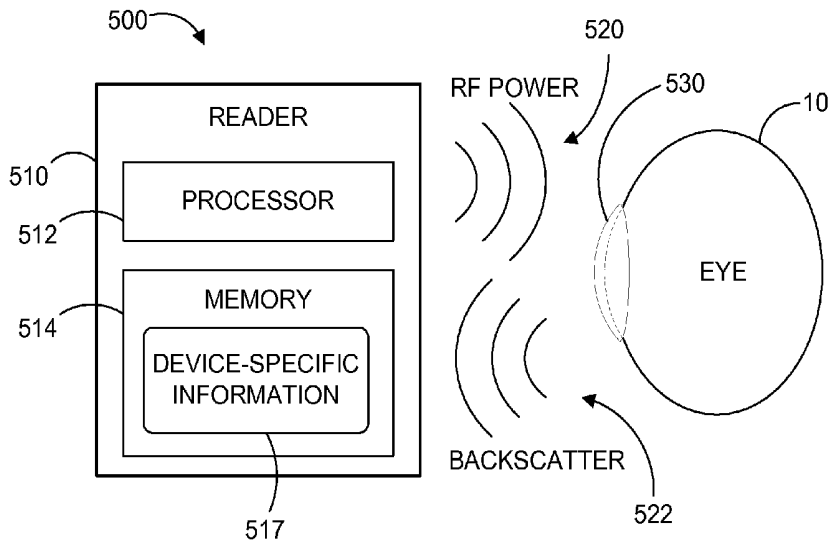
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(57) **ABSTRACT**

An eye-mountable device includes a controller embedded in a polymeric material configured for mounting to a surface of an eye. The controller is electrically connected to an antenna included in the eye-mountable device. The controller is configured to: (i) receive an indication of an interrogation signal via the antenna, (ii) responsive to the interrogation signal, output a substantially unique identification sequence; and (iii) use the antenna to communicate the substantially unique identification sequence. The substantially unique identification sequence can then be used by external readers to associate the eye-mountable device with device-specific information without storing such information on the eye-mountable device.

22 Claims, 11 Drawing Sheets



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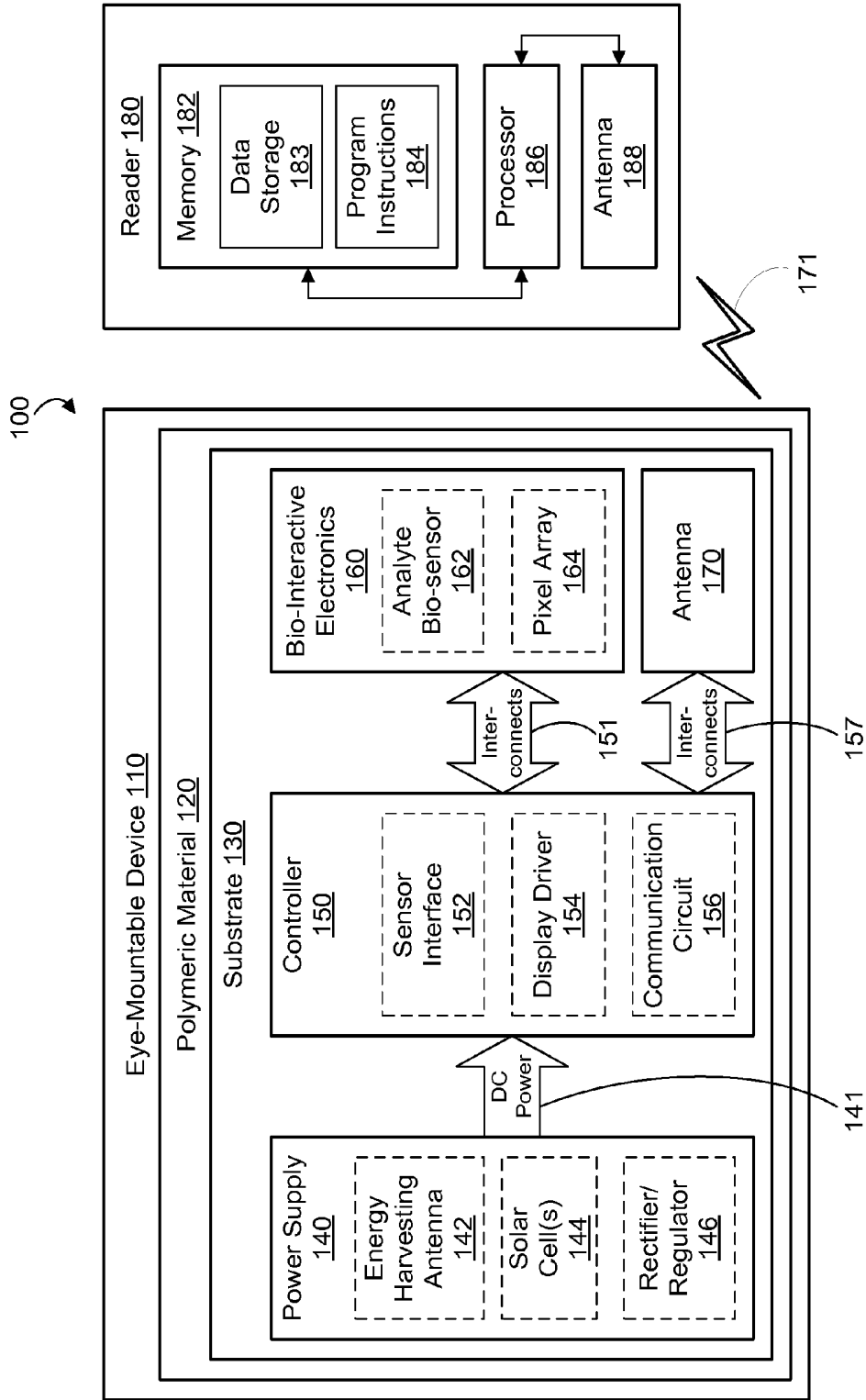


FIG. 1

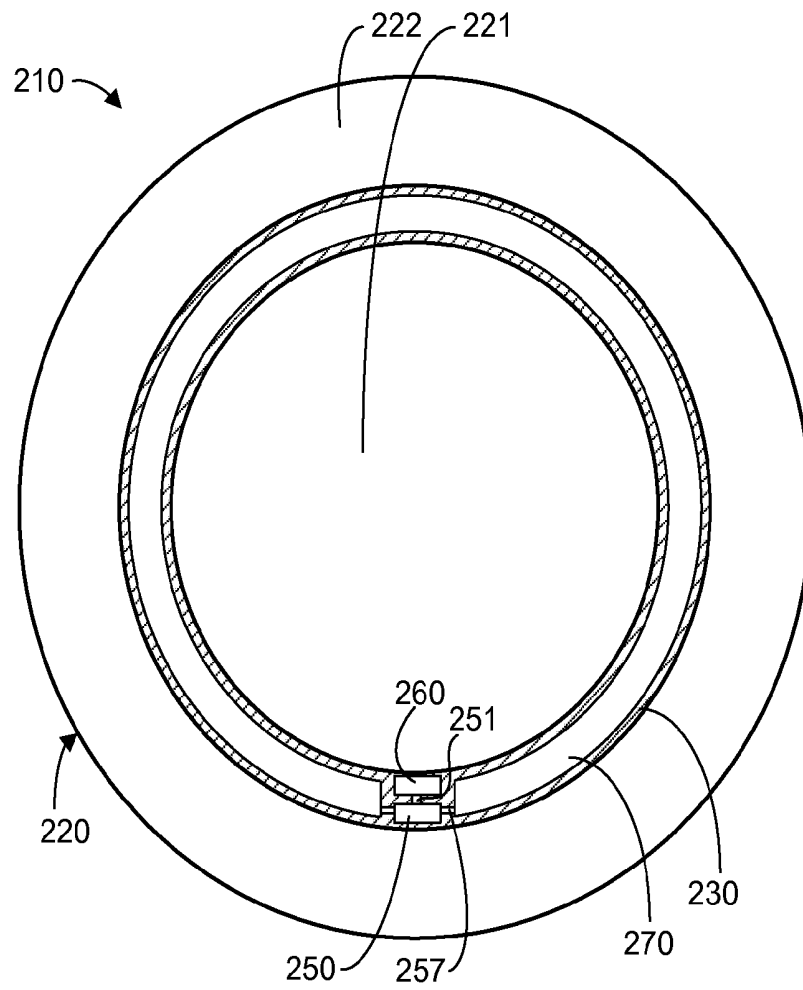


FIG. 2A

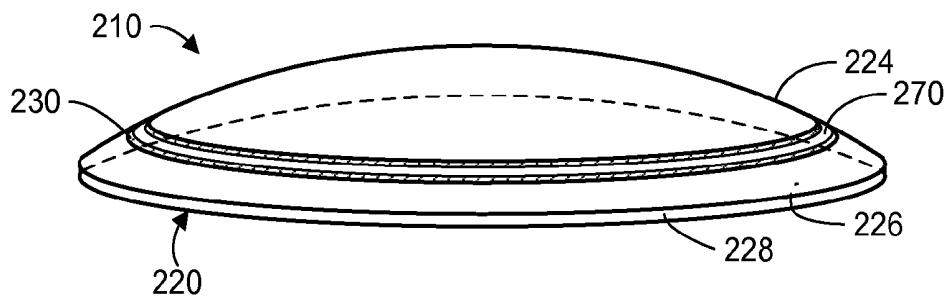


FIG. 2B

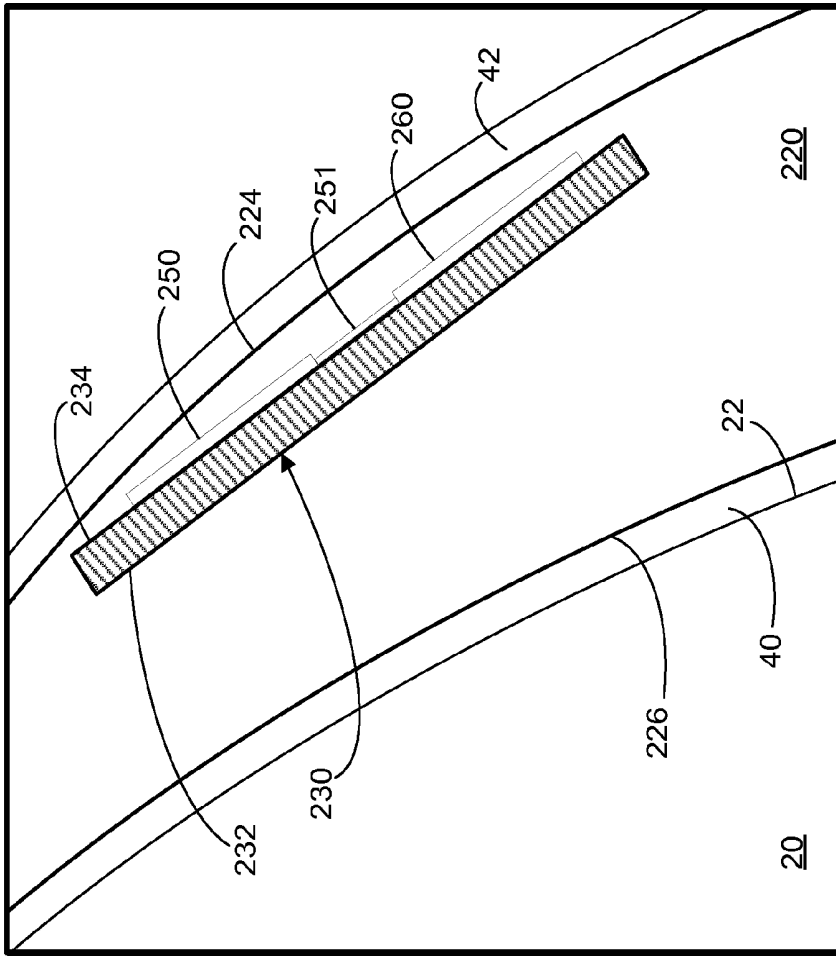


FIG. 2D

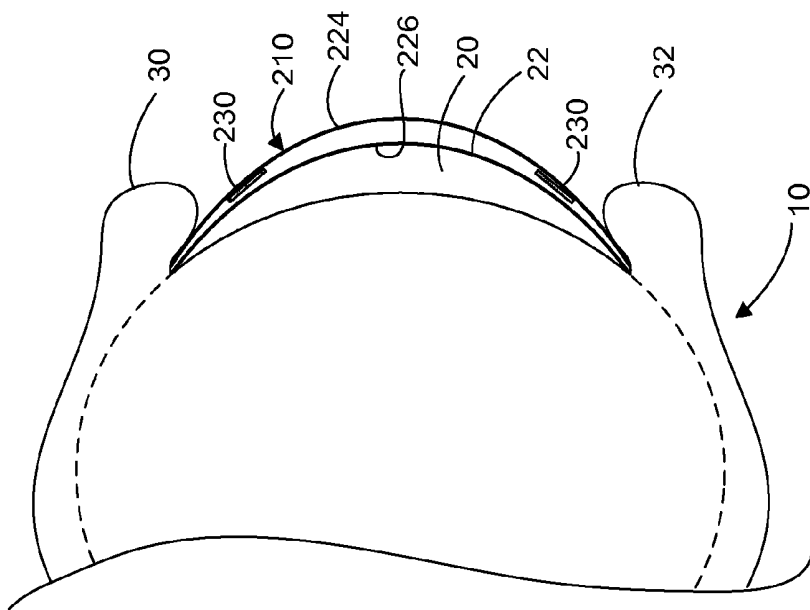


FIG. 2C

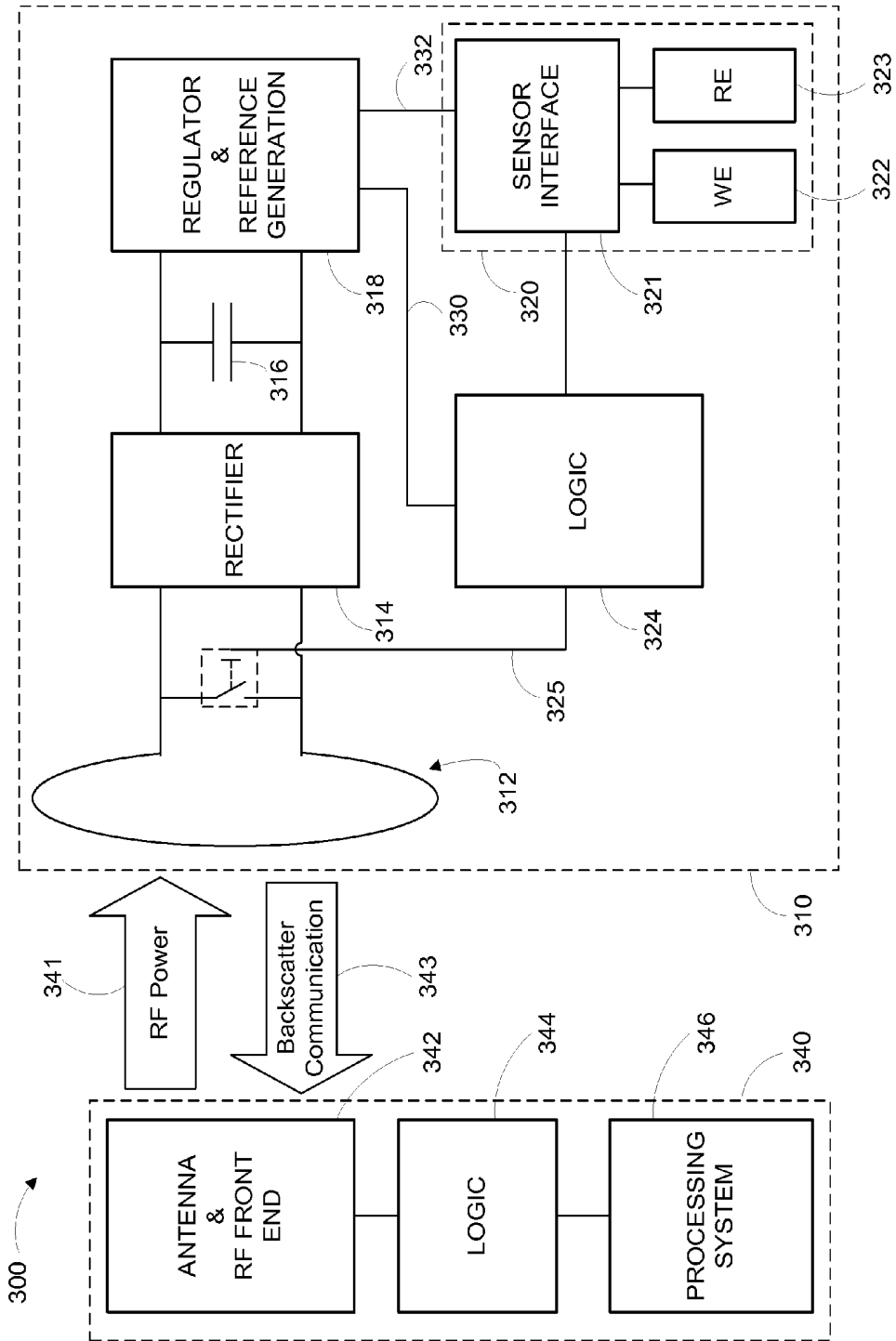


FIG. 3

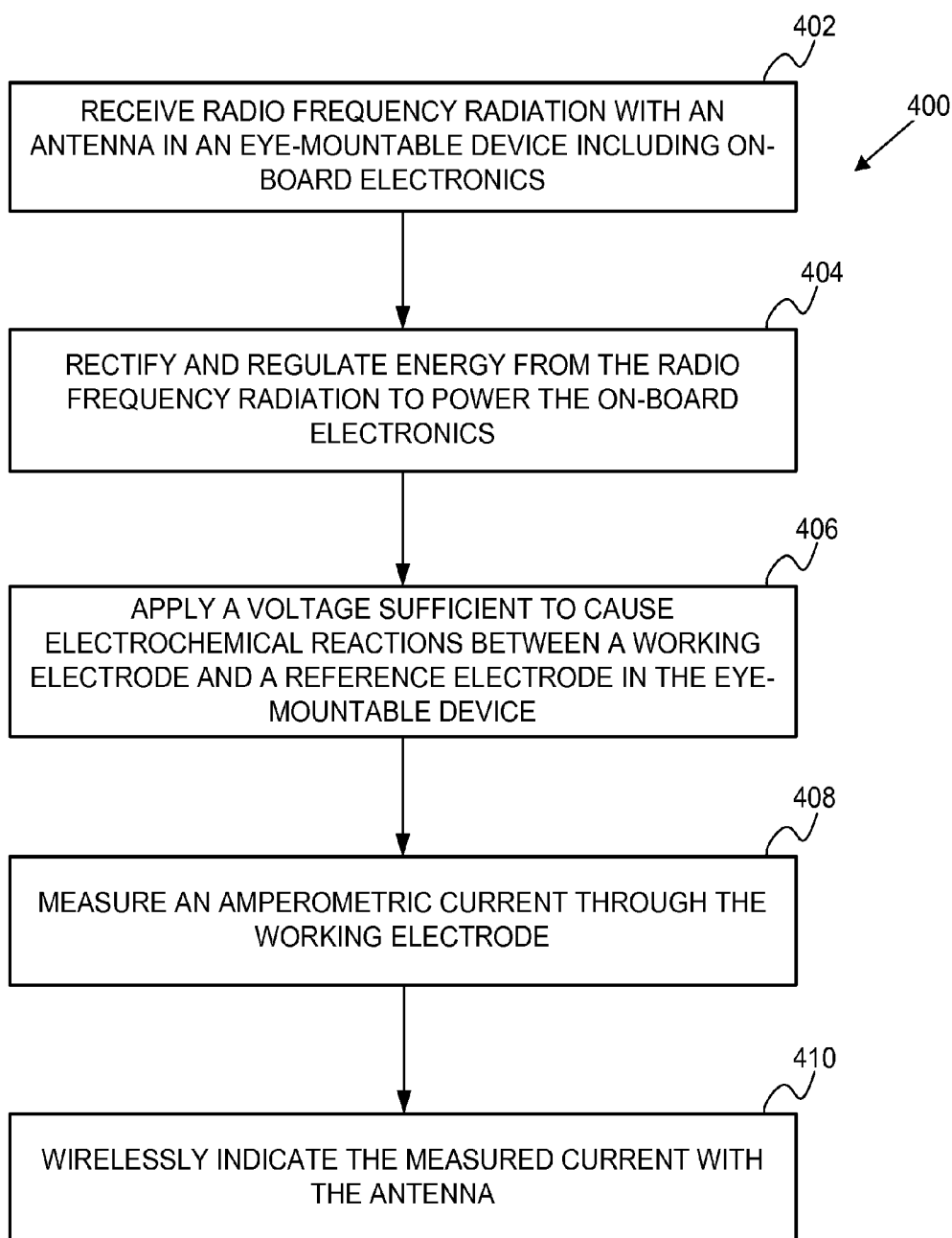
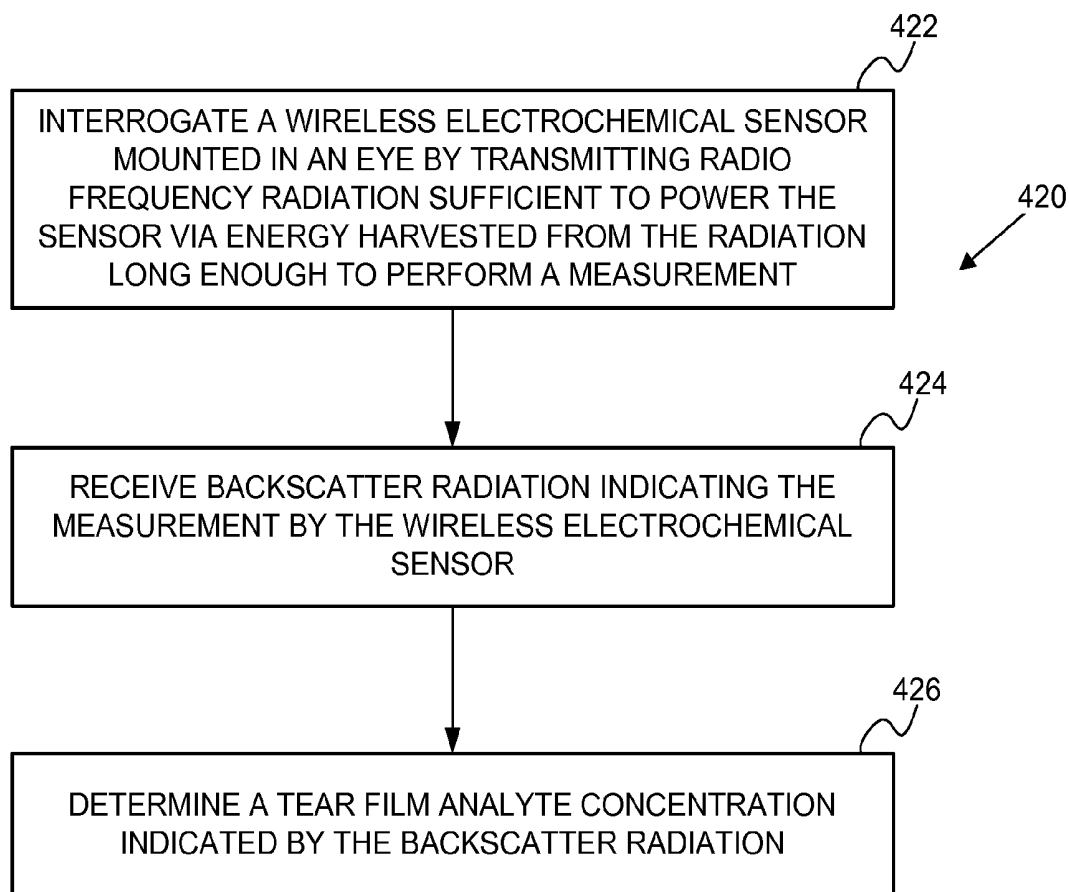


FIG. 4A

**FIG. 4B**

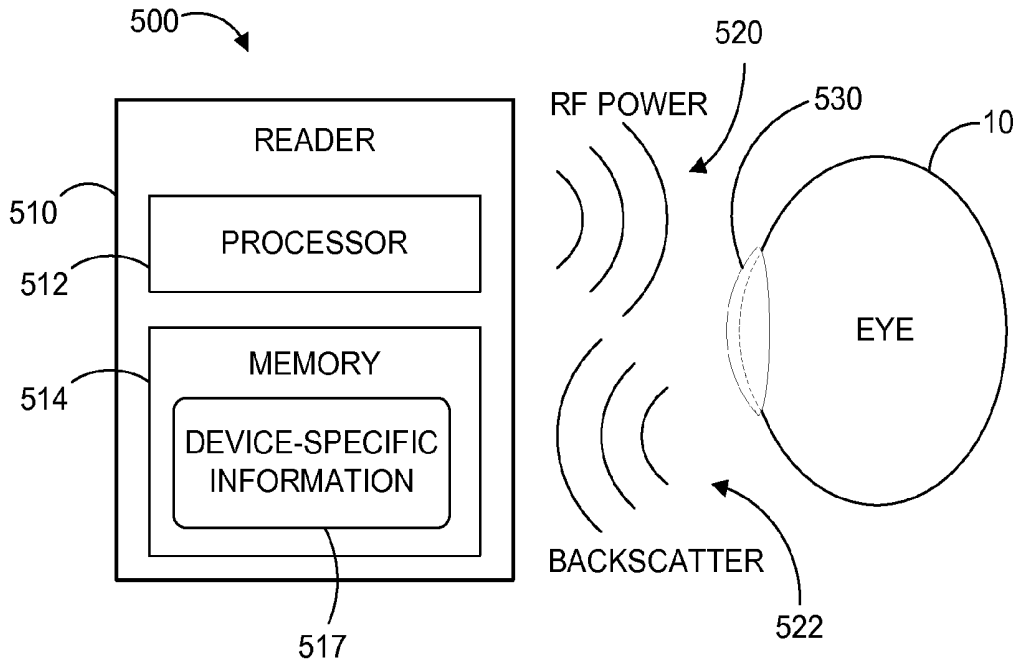


FIG. 5A

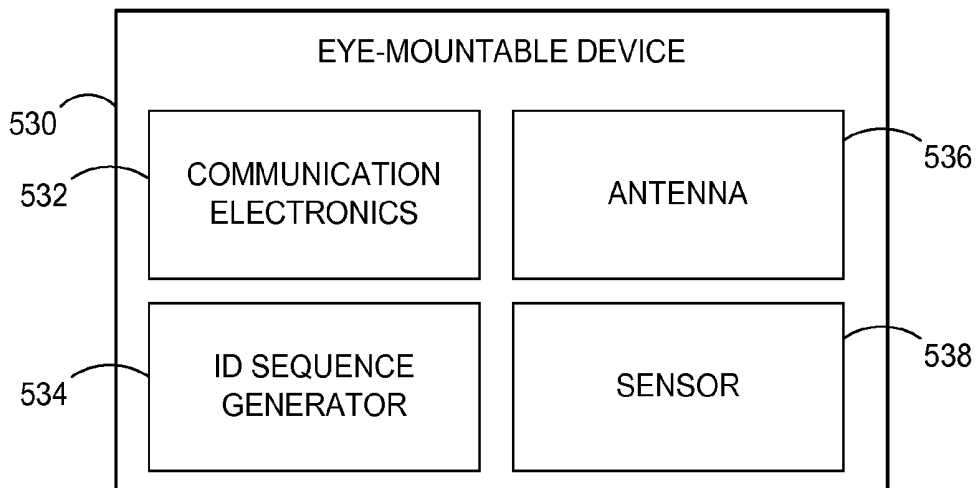


FIG. 5B

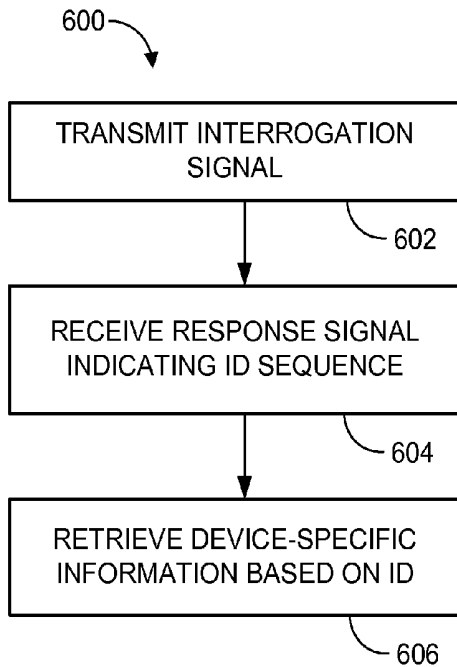


FIG. 6A

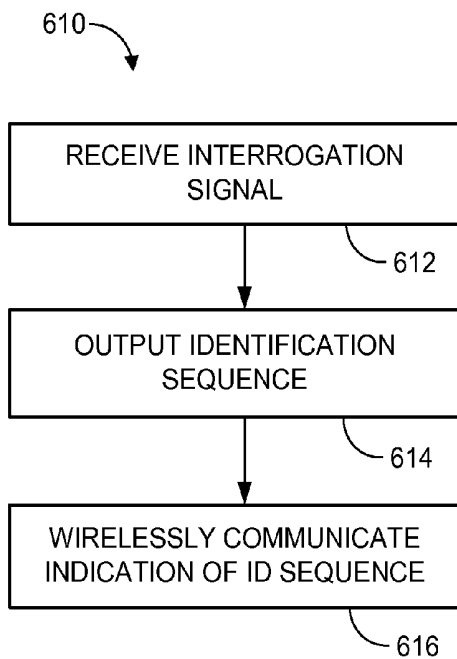


FIG. 6B

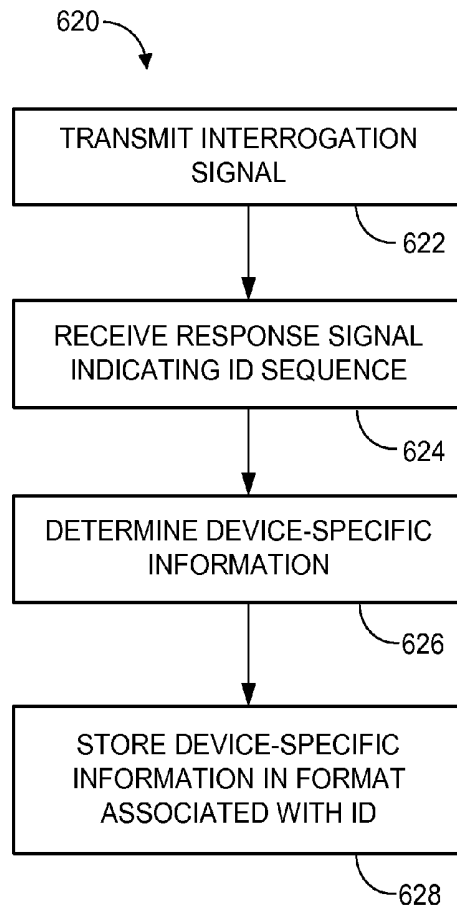


FIG. 6C

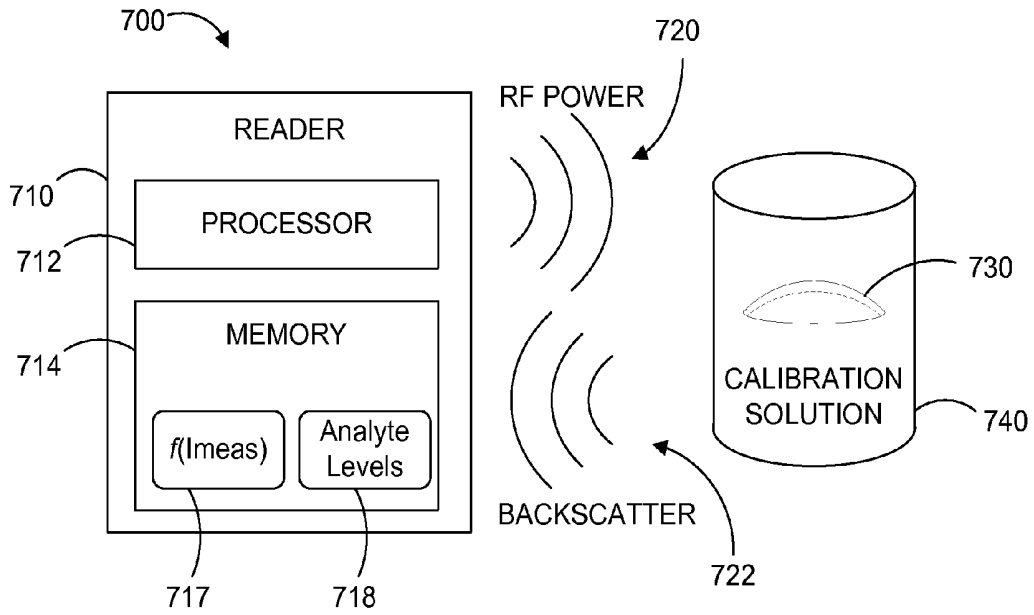


FIG. 7A

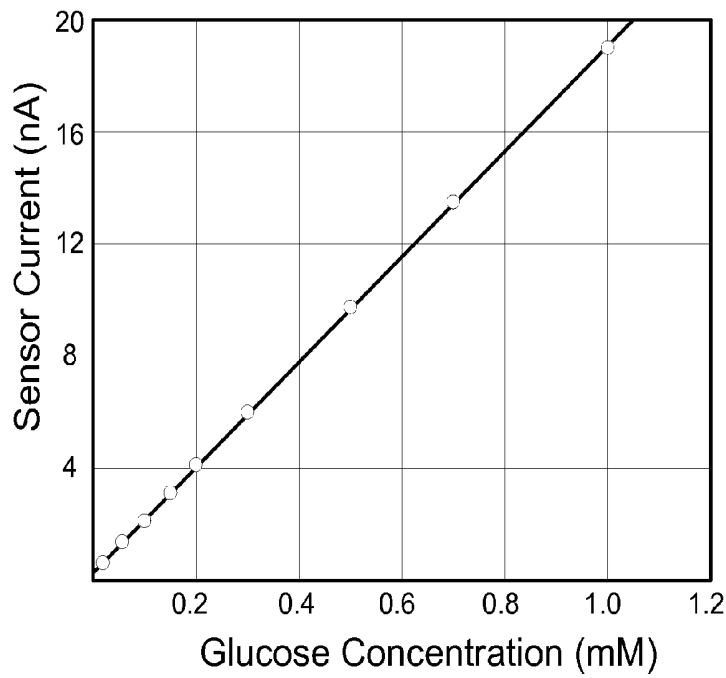


FIG. 7B

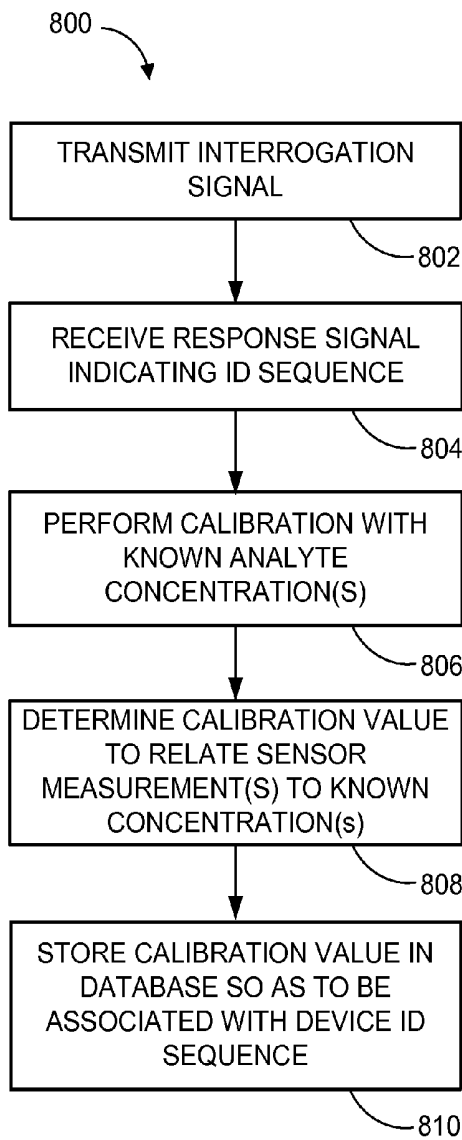


FIG. 8A

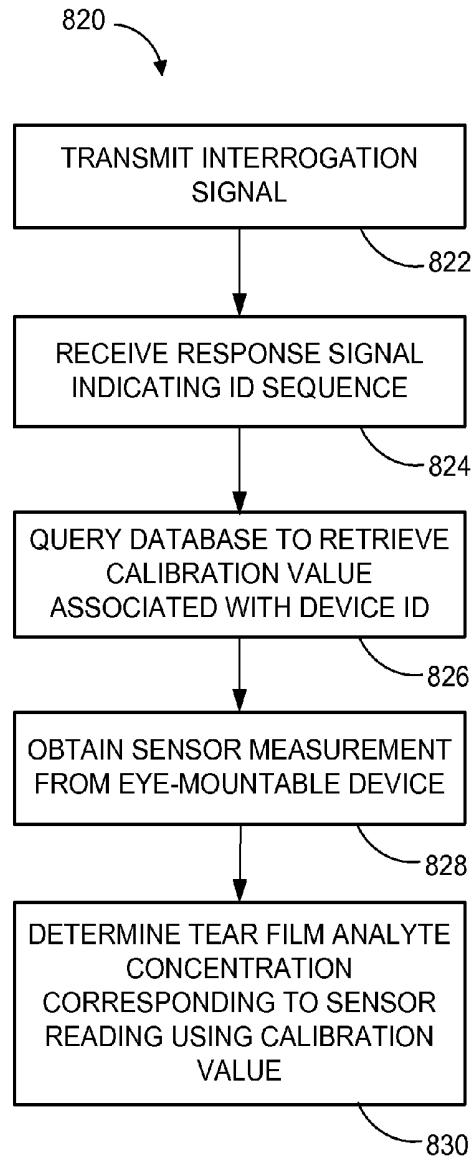


FIG. 8B

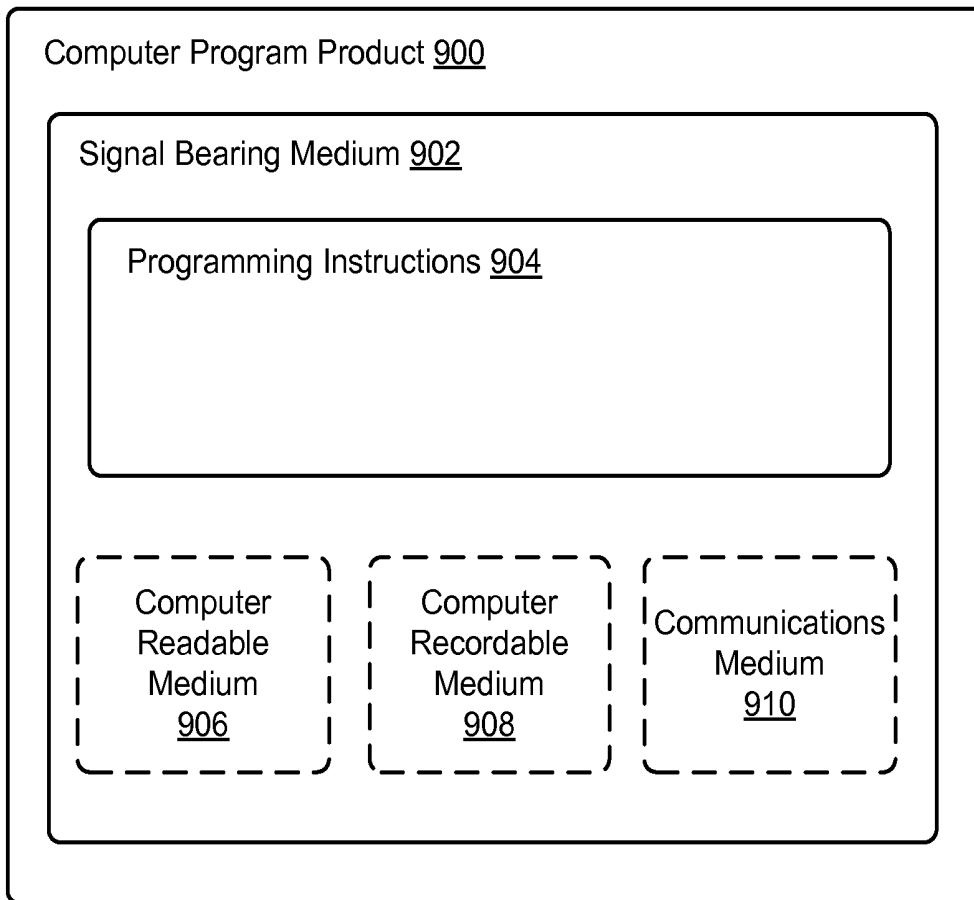


FIG. 9

DEVICE IDENTIFICATION

BACKGROUND

Unless otherwise indicated herein, the materials described in this section are not prior art to the claims in this application and are not admitted to be prior art by inclusion in this section.

An electrochemical amperometric sensor measures a concentration of an analyte by measuring a current generated through electrochemical oxidation or reduction reactions of the analyte at a working electrode of the sensor. A reduction reaction occurs when electrons are transferred from the electrode to the analyte, whereas an oxidation reaction occurs when electrons are transferred from the analyte to the electrode. The direction of the electron transfer is dependent upon the electrical potentials applied to the working electrode. A counter electrode and/or reference electrode is used to complete a circuit with the working electrode and allow the generated current to flow. When the working electrode is appropriately biased, the output current can be proportional to the reaction rate, so as to provide a measure of the concentration of the analyte surrounding the working electrode. Ideally, the output current is linearly related to the actual concentration of the analyte, and the linear relationship can therefore be characterized by a two parameter fit (e.g., slope and intercept).

In some examples, a reagent is localized proximate the working electrode to selectively react with a desired analyte. For example, glucose oxidase can be fixed near the working electrode to react with glucose and release hydrogen peroxide, which is then electrochemically detected by the working electrode to indicate the presence of glucose. Other enzymes and/or reagents can be used to detect other analytes.

SUMMARY

An eye-mountable device includes a controller embedded in a polymeric material configured for mounting to a surface of an eye. The controller is electrically connected to an antenna included in the eye-mountable device. The controller is configured to: (i) receive an indication of an interrogation signal via the antenna, (ii) responsive to the interrogation signal, output a substantially unique identification sequence; and (iii) use the antenna to communicate the substantially unique identification sequence. The substantially unique identification sequence can then be used to associate the eye-mountable device with device-specific information without storing such information on the eye-mountable device. As such, the eye-mountable device can be associated with device-specific information while being free of programmable memory.

Some embodiments of the present disclosure provide an eye-mountable device including a transparent polymeric material, a substrate, an antenna, and a controller. The transparent polymeric material can have a concave surface and a convex surface. The concave surface can be configured to be removably mounted over a corneal surface and the convex surface can be configured to be compatible with eyelid motion when the concave surface is so mounted. The substrate can be at least partially embedded within the transparent polymeric material. The antenna can be disposed on the substrate. The controller can be electrically connected to the antenna and can be configured to: (i) receive an indication of an interrogation signal via the antenna, (ii) responsive to the interrogation signal, output a substantially

unique identification sequence; and (iii) use the antenna to communicate the substantially unique identification sequence.

Some embodiments of the present disclosure provide a method. The method can include transmitting an interrogation signal to an eye-mountable device. The method can include receiving, from the eye-mountable device, a response signal indicative of a substantially unique identification sequence. The method can include associating the eye-mountable device with device-specific information based on the substantially unique identification sequence.

Some embodiments of the present disclosure provide a non-transitory computer readable medium storing instructions that, when executed by one or more processors in a computing device, cause the computing device to perform operations. The operations can include transmitting an interrogation signal to an eye-mountable device. The operations can include receiving, from the eye-mountable device, a response signal indicative of a substantially unique identification sequence. The operations can include associating the eye-mountable device with device-specific information based on the substantially unique identification sequence.

Some embodiments of the present disclosure provide a body-mountable device including a bio-compatible polymeric material, a substrate, an antenna, and a controller. The substrate can be at least partially embedded within the bio-compatible polymeric material. The antenna can be disposed on the substrate. The controller can be electrically connected to the antenna and configured to: (i) receive an indication of an interrogation signal via the antenna, (ii) responsive to the interrogation signal, output a substantially unique identification sequence; and (iii) use the antenna to communicate the substantially unique identification sequence.

Some embodiments include means for transmitting an interrogation signal to an eye-mountable device. Some embodiments include means for receiving, from the eye-mountable device, a response signal indicative of a substantially unique identification sequence. Some embodiments include means for associating the eye-mountable device with device-specific information based on the substantially unique identification sequence.

Some embodiments include means for associating an eye-mountable device with device-specific information without storing information in programmable memory included in the eye-mountable device. Some embodiments include means for implementing an eye-mountable device without including programmable memory.

These as well as other aspects, advantages, and alternatives, will become apparent to those of ordinary skill in the art by reading the following detailed description, with reference where appropriate to the accompanying figures.

BRIEF DESCRIPTION OF THE FIGURES

FIG. 1 is a block diagram of an example system that includes an eye-mountable device in wireless communication with an external reader.

FIG. 2A is a top view of an example eye-mountable device.

FIG. 2B is a side view of the example eye-mountable device shown in FIG. 2A.

FIG. 2C is a side cross-section view of the example eye-mountable device shown in FIGS. 2A and 2B while mounted to a corneal surface of an eye.

FIG. 2D is a side cross-section view enhanced to show the tear film layers surrounding the surfaces of the example eye-mountable device when mounted as shown in FIG. 2C.

FIG. 3 is a functional block diagram of an example system for electrochemically measuring a tear film analyte concentration.

FIG. 4A is a flowchart of an example process for operating an amperometric sensor in an eye-mountable device to measure a tear film analyte concentration.

FIG. 4B is a flowchart of an example process for operating an external reader to interrogate an amperometric sensor in an eye-mountable device to measure a tear film analyte concentration.

FIG. 5A is a block diagram of an example eye-mountable electronics platform in communication with an external reader.

FIG. 5B is a block diagram of the example eye-mountable electronics platform described in connection with FIG. 5A.

FIG. 6A is a flowchart of an example process for retrieving device-specific information based on an identification sequence for an eye-mountable device.

FIG. 6B is a flowchart of an example process for communicating an identification sequence from an eye-mountable device.

FIG. 6C is a flowchart of an example process for storing device-specific information for an eye-mountable device.

FIG. 7A is a block diagram of an example ophthalmic analyte sensor undergoing calibration.

FIG. 7B is a graph showing example amperometric current values for a range of glucose concentrations.

FIG. 8A is a flowchart of an example process for calibrating an ophthalmic analyte sensor.

FIG. 8B is a flowchart of an example process for interpreting a sensor reading using a predetermined calibration value.

FIG. 9 depicts a computer-readable medium configured according to an example embodiment.

DETAILED DESCRIPTION

In the following detailed description, reference is made to the accompanying figures, which form a part hereof. In the figures, similar symbols typically identify similar components, unless context dictates otherwise. The illustrative embodiments described in the detailed description, figures, and claims are not meant to be limiting. Other embodiments may be utilized, and other changes may be made, without departing from the scope of the subject matter presented herein. It will be readily understood that the aspects of the present disclosure, as generally described herein, and illustrated in the figures, can be arranged, substituted, combined, separated, and designed in a wide variety of different configurations, all of which are explicitly contemplated herein.

I. Overview

An ophthalmic sensing platform or implantable sensing platform can include a sensor, control electronics and an antenna all situated on a substrate embedded in a polymeric material. The polymeric material can be incorporated in an ophthalmic device, such as an eye-mountable device or an implantable medical device. The control electronics can operate the sensor to perform readings and can operate the antenna to wirelessly communicate the readings from the sensor to an external reader via the antenna. The sensing platform can be configured to output a substantially unique identification sequence and communicate the sequence to the reader. The reader can then identify a particular device based on the identification sequence, and associate device-

specific information with the particular device. As such, any device-specific information, such as configuration/calibration data and the like can be stored in the reader (or a database in accessible by the reader), and the sensing platform can be implemented without any programmable memory.

The polymeric material can be in the form of a round lens with a concave curvature configured to mount to a corneal surface of an eye. An opposing convex surface can be configured to avoid interference with eyelid motion while the eye-mountable device is mounted to the eye. The substrate, and electronics components mounted thereon, can be embedded near the periphery of the polymeric material to avoid interference with incident light received closer to the central region of the cornea. The eye-mountable device can be powered via harvested energy received by the eye-mountable device. For example, the device can be powered by photovoltaic cells included on the sensing platform that are energized by incident light. Additionally or alternatively, power can be provided by radio frequency energy inductively harvested using the antenna. For example, power can be provided by rectifying voltage variations on the leads of the antenna from energy received via an electromagnetic coupling. A rectifier and/or regulator can be incorporated with the control electronics to generate a stable DC voltage to power the remaining electronics components. The antenna can be arranged as a loop of conductive material with leads connected to the control electronics. In some embodiments, such a loop antenna can also wirelessly communicate with an external reader by modifying the impedance of the loop antenna so as to characteristically modify backscatter radiation from the antenna. In some embodiments, the loop antenna, or a second antenna either on the substrate or included in the control chip, may actively broadcast a signal to be received by an external reader. Such active broadcast may be in addition to, or as an alternative to, modulated backscatter radiation from an energy-harvesting antenna.

Tear fluid contains a variety of inorganic electrolytes (e.g., Ca^{2+} , Mg^{2+} , Cl^-), organic components (e.g., glucose, lactate, proteins, lipids, etc.), and so on that can be used to diagnose health states. The eye-mountable device may include an electrochemical amperometric sensor or another bio-sensor configured to measure concentrations of one or more analytes. An eye-mountable device configured to measure one or more of these analytes can thus provide a convenient non-invasive platform useful in diagnosing and/or monitoring health states. For example, an eye-mountable device can be configured to sense glucose and can be used by diabetic individuals to measure/monitor their glucose levels.

The eye-mountable device, and associated reader, can operate to repeatedly obtain measurements and communicate the results back to the reader. The eye-mountable device can obtain measurements and transmit responsive signals to the reader whenever it receives sufficient radio frequency radiation to power the sensor platform to turn on via inductively harvested energy.

The eye-mountable device can be implemented without on-board programmable memory. Instead, device-specific information such as calibration information (or other configuration information), historical sensor readings (or other user-specific information) can be stored in the external reader or in a database accessible to the reader. Device-specific information may also include, for example, thresholds for alerts related to sensor data readings, user preferences, configuration settings. For example, the device-specific information may specify the sampling frequency for

a biosensor included in the eye-mountable device (or other conditions of the operation of the biosensor). To associate such device-specific information with a particular eye-mountable device, the eye-mountable device can be configured to generate and output a distinctive signature, such as a substantially unique identification sequence. The identification sequence can be communicated to the reader, which can then associate a particular eye-mountable device with corresponding device-specific information using the substantially unique identification sequence to distinguish between different eye-mountable devices. The substantially unique identification sequence can be a data series that can be repeatedly (i.e., consistently) generated by the eye-mountable device in response to an interrogation signal. In some cases, the data series is hard-coded into the control electronics of the eye-mountable device (e.g., during device manufacture) akin to a serial number. In some cases, the data series is generated dynamically (but repeatably) in accordance with process variations in a series of circuit components. For instance, a series of binary bits can be constructed from the output of a set of comparator circuits that each settle in one state or another depending on the difference in threshold voltage between two TFTs.

For eye-mountable devices equipped with electrochemical bio-sensors, device-specific information can include sensor calibration information. The calibration information may be related to interpreting results (e.g., current offsets, current/voltage slope information, etc.). Such calibration information can then be used by the reader in interpreting the sensor readings as indications of analyte levels (e.g., mapping sensor readings to analyte concentrations). The calibration information may be based on a manufacturing batch of a particular eye-mountable device. Additionally or alternatively, calibration information may be based on previously obtained calibration results for a particular eye-mountable device. The device-specific information may additionally or alternatively include sensor configuration information and/or user preferences for operating the sensor (e.g., voltage offset settings, sensor stabilization durations, measurement frequencies, etc.). Such configuration information can then be used to cause the eye-mountable device to obtain measurements in accordance with the configuration information. For example, an indication of sensor stabilization time can cause the reader to initiate a stabilization operation prior to obtaining a sensor measurement with a duration specified in the configuration information.

Configuring the eye-mountable device without programmable memory, and instead storing device-specific information in the external reader or in a database accessible to the external reader, allows the eye-mountable device to operate at a reduced power budget. Historical sensor readings for a particular user can also be loaded to an external reader or database to allow the user to track their readings over time, without relying on the resiliency/longevity of any one particular eye-mountable device, which may be disposable. In addition, such eye-mountable devices can be disposed without losing any user-specific or user-sensitive information (e.g., bio-sensor measurements), because such information is stored only on the external reader and/or networked database.

II. Example Ophthalmic Electronics Platform

FIG. 1 is a block diagram of a system 100 that includes an eye-mountable device 110 in wireless communication with an external reader 180. The exposed regions of the eye-mountable device 110 are made of a polymeric material 120 formed to be contact-mounted to a corneal surface of an eye. A substrate 130 is embedded in the polymeric material

120 to provide a mounting surface for a power supply 140, a controller 150, bio-interactive electronics 160, and a communication antenna 170. The bio-interactive electronics 160 are operated by the controller 150. The power supply 140 supplies operating voltages to the controller 150 and/or the bio-interactive electronics 160. The antenna 170 is operated by the controller 150 to communicate information to and/or from the eye-mountable device 110. The antenna 170, the controller 150, the power supply 140, and the bio-interactive electronics 160 can all be situated on the embedded substrate 130. Because the eye-mountable device 110 includes electronics and is configured to be contact-mounted to an eye, it is also referred to herein as an ophthalmic electronics platform.

To facilitate contact-mounting, the polymeric material 120 can have a concave surface configured to adhere (“mount”) to a moistened corneal surface (e.g., by capillary forces with a tear film coating the corneal surface). Additionally or alternatively, the eye-mountable device 110 can be adhered by a vacuum force between the corneal surface and the polymeric material due to the concave curvature. While mounted with the concave surface against the eye, the outward-facing surface of the polymeric material 120 can have a convex curvature that is formed to not interfere with eye-lid motion while the eye-mountable device 110 is mounted to the eye. For example, the polymeric material 120 can be a substantially transparent curved polymeric disk shaped similarly to a contact lens.

The polymeric material 120 can include one or more biocompatible materials, such as those employed for use in contact lenses or other ophthalmic applications involving direct contact with the corneal surface. The polymeric material 120 can optionally be formed in part from such biocompatible materials or can include an outer coating with such biocompatible materials. The polymeric material 120 can include materials configured to moisturize the corneal surface, such as hydrogels and the like. In some embodiments, the polymeric material 120 can be a deformable (“non-rigid”) material to enhance wearer comfort. In some embodiments, the polymeric material 120 can be shaped to provide a predetermined, vision-correcting optical power, such as can be provided by a contact lens.

The substrate 130 includes one or more surfaces suitable for mounting the bio-interactive electronics 160, the controller 150, the power supply 140, and the antenna 170. The substrate 130 can be employed both as a mounting platform for chip-based circuitry (e.g., by flip-chip mounting to connection pads) and/or as a platform for patterning conductive materials (e.g., gold, platinum, palladium, titanium, copper, aluminum, silver, metals, other conductive materials, combinations of these, etc.) to create electrodes, interconnects, connection pads, antennae, etc. In some embodiments, substantially transparent conductive materials (e.g., indium tin oxide) can be patterned on the substrate 130 to form circuitry, electrodes, etc. For example, the antenna 170 can be formed by forming a pattern of gold or another conductive material on the substrate 130 by deposition, photolithography, electroplating, etc. Similarly, interconnects 151, 157 between the controller 150 and the bio-interactive electronics 160, and between the controller 150 and the antenna 170, respectively, can be formed by depositing suitable patterns of conductive materials on the substrate 130. A combination of microfabrication techniques including, without limitation, the use of photoresists, masks, deposition techniques, and/or plating techniques can be employed to pattern materials on the substrate 130. The substrate 130 can be a relatively rigid material, such as

polyethylene terephthalate (“PET”) or another material configured to structurally support the circuitry and/or chip-based electronics within the polymeric material **120**. The eye-mountable device **110** can alternatively be arranged with a group of unconnected substrates rather than a single substrate. For example, the controller **150** and a bio-sensor or other bio-interactive electronic component can be mounted to one substrate, while the antenna **170** is mounted to another substrate and the two can be electrically connected via the interconnects **157**.

In some embodiments, the bio-interactive electronics **160** (and the substrate **130**) can be positioned away from the center of the eye-mountable device **110** and thereby avoid interference with light transmission to the central, light-sensitive region of the eye. For example, where the eye-mountable device **110** is shaped as a concave-curved disk, the substrate **130** can be embedded around the periphery (e.g., near the outer circumference) of the disk. In some embodiments, however, the bio-interactive electronics **160** (and the substrate **130**) can be positioned in or near the central region of the eye-mountable device **110**. Additionally or alternatively, the bio-interactive electronics **160** and/or substrate **130** can be substantially transparent to incoming visible light to mitigate interference with light transmission to the eye. Moreover, in some embodiments, the bio-interactive electronics **160** can include a pixel array **164** that emits and/or transmits light to be received by the eye according to display instructions. Thus, the bio-interactive electronics **160** can optionally be positioned in the center of the eye-mountable device so as to generate perceivable visual cues to a wearer of the eye-mountable device **110**, such as by displaying information (e.g., characters, symbols, flashing patterns, etc.) on the pixel array **164**.

The substrate **130** can be shaped as a flattened ring with a radial width dimension sufficient to provide a mounting platform for the embedded electronics components. The substrate **130** can have a thickness sufficiently small to allow the substrate **130** to be embedded in the polymeric material **120** without influencing the profile of the eye-mountable device **110**. The substrate **130** can have a thickness sufficiently large to provide structural stability suitable for supporting the electronics mounted thereon. For example, the substrate **130** can be shaped as a ring with a diameter of about 10 millimeters, a radial width of about 1 millimeter (e.g., an outer radius 1 millimeter larger than an inner radius), and a thickness of about 50 micrometers. The substrate **130** can optionally be aligned with the curvature of the eye-mounting surface of the eye-mountable device **110** (e.g., convex surface). For example, the substrate **130** can be shaped along the surface of an imaginary cone between two circular segments that define an inner radius and an outer radius. In such an example, the surface of the substrate **130** along the surface of the imaginary cone defines an inclined surface that is approximately aligned with the curvature of the eye mounting surface at that radius.

The power supply **140** is configured to harvest ambient energy to power the controller **150** and bio-interactive electronics **160**. For example, a radio-frequency energy-harvesting antenna **142** can capture energy from incident radio radiation. Additionally or alternatively, solar cell(s) **144** (“photovoltaic cells”) can capture energy from incoming ultraviolet, visible, and/or infrared radiation. Furthermore, an inertial power scavenging system can be included to capture energy from ambient vibrations. The energy harvesting antenna **142** can optionally be a dual-purpose antenna that is also used to communicate information to the external reader **180**. That is, the functions of the communi-

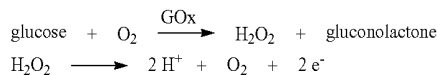
cation antenna **170** and the energy harvesting antenna **142** can be accomplished with the same physical antenna.

A rectifier/regulator **146** can be used to condition the captured energy to a stable DC supply voltage **141** that is supplied to the controller **150**. For example, the energy harvesting antenna **142** can receive incident radio frequency radiation. Varying electrical signals on the leads of the antenna **142** are output to the rectifier/regulator **146**. The rectifier/regulator **146** rectifies the varying electrical signals to a DC voltage and regulates the rectified DC voltage to a level suitable for operating the controller **150**. Additionally or alternatively, output voltage from the solar cell(s) **144** can be regulated to a level suitable for operating the controller **150**. The rectifier/regulator **146** can include one or more energy storage devices to mitigate high frequency variations in the ambient energy gathering antenna **142** and/or solar cell(s) **144**. For example, one or more energy storage devices (e.g., a capacitor, an inductor, etc.) can be connected in parallel across the outputs of the rectifier **146** to regulate the DC supply voltage **141** and configured to function as a low-pass filter.

The controller **150** is turned on when the DC supply voltage **141** is provided to the controller **150**, and the logic in the controller **150** operates the bio-interactive electronics **160** and the antenna **170**. The controller **150** can include logic circuitry configured to operate the bio-interactive electronics **160** so as to interact with a biological environment of the eye-mountable device **110**. The interaction could involve the use of one or more components, such as an analyte bio-sensor **162**, in bio-interactive electronics **160** to obtain input from the biological environment. Additionally or alternatively, the interaction could involve the use of one or more components, such as pixel array **164**, to provide an output to the biological environment.

In one example, the controller **150** includes a sensor interface module **152** that is configured to operate analyte bio-sensor **162**. The analyte bio-sensor **162** can be, for example, an amperometric electrochemical sensor that includes a working electrode and a reference electrode. A voltage can be applied between the working and reference electrodes to cause an analyte to undergo an electrochemical reaction (e.g., a reduction and/or oxidation reaction) at the working electrode. The electrochemical reaction can generate an amperometric current that can be measured through the working electrode. The amperometric current can be dependent on the analyte concentration. Thus, the amount of the amperometric current that is measured through the working electrode can provide an indication of analyte concentration. In some embodiments, the sensor interface module **152** can be a potentiostat configured to apply a voltage difference between working and reference electrodes while measuring a current through the working electrode.

In some instances, a reagent can also be included to sensitize the electrochemical sensor to one or more desired analytes. For example, a layer of glucose oxidase (“GOx”) proximal to the working electrode can catalyze glucose oxidation to generate hydrogen peroxide (H₂O₂). The hydrogen peroxide can then be electro-oxidized at the working electrode, which releases electrons to the working electrode, resulting in an amperometric current that can be measured through the working electrode.



The current generated by either reduction or oxidation reactions is approximately proportionate to the reaction rate. Further, the reaction rate is dependent on the rate of analyte molecules reaching the electrochemical sensor electrodes to fuel the reduction or oxidation reactions, either directly or catalytically through a reagent. In a steady state, where analyte molecules diffuse to the electrochemical sensor electrodes from a sampled region at approximately the same rate that additional analyte molecules diffuse to the sampled region from surrounding regions, the reaction rate is approximately proportionate to the concentration of the analyte molecules. The current measured through the working electrode thus provides an indication of the analyte concentration.

The controller **150** can optionally include a display driver module **154** for operating a pixel array **164**. The pixel array **164** can be an array of separately programmable light transmitting, light reflecting, and/or light emitting pixels arranged in rows and columns. The individual pixel circuits can optionally include liquid crystal technologies, micro-electromechanical technologies, emissive diode technologies, etc. to selectively transmit, reflect, and/or emit light according to information from the display driver module **154**. Such a pixel array **164** can also optionally include more than one color of pixels (e.g., red, green, and blue pixels) to render visual content in color. The display driver module **154** can include, for example, one or more data lines providing programming information to the separately programmed pixels in the pixel array **164** and one or more addressing lines for setting groups of pixels to receive such programming information. Such a pixel array **164** situated on the eye can also include one or more lenses to direct light from the pixel array to a focal plane perceivable by the eye.

The controller **150** can also include a communication circuit **156** for sending and/or receiving information via the antenna **170**. The communication circuit **156** can optionally include one or more oscillators, mixers, frequency injectors, etc. to modulate and/or demodulate information on a carrier frequency to be transmitted and/or received by the antenna **170**. In some examples, the eye-mountable device **110** is configured to indicate an output from a bio-sensor by modulating an impedance of the antenna **170** in a manner that is perceivable by the external reader **180**. For example, the communication circuit **156** can cause variations in the amplitude, phase, and/or frequency of backscatter radiation from the antenna **170**, and such variations can be detected by the reader **180**.

The controller **150** is connected to the bio-interactive electronics **160** via interconnects **151**. For example, where the controller **150** includes logic elements implemented in an integrated circuit to form the sensor interface module **152** and/or display driver module **154**, a patterned conductive material (e.g., gold, platinum, palladium, titanium, copper, aluminum, silver, metals, combinations of these, etc.) can connect a terminal on the chip to the bio-interactive electronics **160**. Similarly, the controller **150** is connected to the antenna **170** via interconnects **157**.

It is noted that the block diagram shown in FIG. **1** is described in connection with functional modules for convenience in description. However, embodiments of the eye-mountable device **110** can be arranged with one or more of the functional modules ("sub-systems") implemented in a single chip, integrated circuit, and/or physical component. For example, while the rectifier/regulator **146** is illustrated in the power supply block **140**, the rectifier/regulator **146** can be implemented in a chip that also includes the logic elements of the controller **150** and/or other features of the

embedded electronics in the eye-mountable device **110**. Thus, the DC supply voltage **141** that is provided to the controller **150** from the power supply **140** can be a supply voltage that is provided to components on a chip by rectifier and/or regulator components located on the same chip. That is, the functional blocks in FIG. **1** shown as the power supply block **140** and controller block **150** need not be implemented as physically separated modules. Moreover, one or more of the functional modules described in FIG. **1** can be implemented by separately packaged chips electrically connected to one another.

Additionally or alternatively, the energy harvesting antenna **142** and the communication antenna **170** can be implemented with the same physical antenna. For example, a loop antenna can both harvest incident radiation for power generation and communicate information via backscatter radiation.

The external reader **180** includes an antenna **188** (or a group of more than one antennae) to send and receive wireless signals **171** to and from the eye-mountable device **110**. The external reader **180** also includes a computing system with a processor **186** in communication with a memory **182**. The memory **182** is a non-transitory computer-readable medium that can include, without limitation, magnetic disks, optical disks, organic memory, and/or any other volatile (e.g. RAM) or non-volatile (e.g. ROM) storage system readable by the processor **186**. The memory **182** can include a data storage **183** to store indications of data, such as sensor readings (e.g., from the analyte bio-sensor **162**), program settings (e.g., to adjust behavior of the eye-mountable device **110** and/or external reader **180**), etc. The memory **182** can also include program instructions **184** for execution by the processor **186** to cause the external reader **180** to perform processes specified by the instructions **184**. For example, the program instructions **184** can cause external reader **180** to provide a user interface that allows for retrieving information communicated from the eye-mountable device **110** (e.g., sensor outputs from the analyte bio-sensor **162**). The external reader **180** can also include one or more hardware components for operating the antenna **188** to send and receive the wireless signals **171** to and from the eye-mountable device **110**. For example, oscillators, frequency injectors, encoders, decoders, amplifiers, filters, etc. can drive the antenna **188** according to instructions from the processor **186**.

The external reader **180** can be a smart phone, digital assistant, or other portable computing device with wireless connectivity sufficient to provide the wireless communication link **171**. The external reader **180** can also be implemented as an antenna module that can be plugged in to a portable computing device, such as in an example where the communication link **171** operates at carrier frequencies not commonly employed in portable computing devices. In some instances, the external reader **180** is a special-purpose device configured to be worn relatively near a wearer's eye to allow the wireless communication link **171** to operate with a low power budget. For example, the external reader **180** can be integrated in a piece of jewelry such as a necklace, earring, etc. or integrated in an article of clothing worn near the head, such as a hat, headband, etc.

In an example where the eye-mountable device **110** includes an analyte bio-sensor **162**, the system **100** can be operated to monitor the analyte concentration in tear film on the surface of the eye. Thus, the eye-mountable device **110** can be configured as a platform for an ophthalmic analyte bio-sensor. The tear film is an aqueous layer secreted from the lacrimal gland to coat the eye. The tear film is in contact

with the blood supply through capillaries in the structure of the eye and includes many biomarkers found in blood that are analyzed to characterize a person's health condition(s). For example, the tear film includes glucose, calcium, sodium, cholesterol, potassium, other biomarkers, etc. The biomarker concentrations in the tear film can be systematically different than the corresponding concentrations of the biomarkers in the blood, but a relationship between the two concentration levels can be established to map tear film biomarker concentration values to blood concentration levels. For example, the tear film concentration of glucose can be established (e.g., empirically determined) to be approximately one tenth the corresponding blood glucose concentration. Although another ratio relationship and/or a non-ratio relationship may be used. Thus, measuring tear film analyte concentration levels provides a non-invasive technique for monitoring biomarker levels in comparison to blood sampling techniques performed by lancing a volume of blood to be analyzed outside a person's body. Moreover, the ophthalmic analyte bio-sensor platform disclosed here can be operated substantially continuously to enable real time monitoring of analyte concentrations.

To perform a reading with the system 100 configured as a tear film analyte monitor, the external reader 180 can emit radio frequency radiation 171 that is harvested to power the eye-mountable device 110 via the power supply 140. Radio frequency electrical signals captured by the energy harvesting antenna 142 (and/or the communication antenna 170) are rectified and/or regulated in the rectifier/regulator 146 and a regulated DC supply voltage 147 is provided to the controller 150. The radio frequency radiation 171 thus turns on the electronic components within the eye-mountable device 110. Once turned on, the controller 150 operates the analyte bio-sensor 162 to measure an analyte concentration level. For example, the sensor interface module 152 can apply a voltage between a working electrode and a reference electrode in the analyte bio-sensor 162. The applied voltage can be sufficient to cause the analyte to undergo an electrochemical reaction at the working electrode and thereby generate an amperometric current that can be measured through the working electrode. The measured amperometric current can provide the sensor reading ("result") indicative of the analyte concentration. The controller 150 can operate the antenna 170 to communicate the sensor reading back to the external reader 180 (e.g., via the communication circuit 156). The sensor reading can be communicated by, for example, modulating an impedance of the communication antenna 170 such that the modulation in impedance is detected by the external reader 180. The modulation in antenna impedance can be detected by, for example, backscatter radiation from the antenna 170.

In some embodiments, the system 100 can operate to non-continuously ("intermittently") supply energy to the eye-mountable device 110 to power the controller 150 and electronics 160. For example, radio frequency radiation 171 can be supplied to power the eye-mountable device 110 long enough to carry out a tear film analyte concentration measurement and communicate the results. For example, the supplied radio frequency radiation can provide sufficient power to apply a potential between a working electrode and a reference electrode sufficient to induce electrochemical reactions at the working electrode, measure the resulting amperometric current, and modulate the antenna impedance to adjust the backscatter radiation in a manner indicative of the measured amperometric current. In such an example, the supplied radio frequency radiation 171 can be considered an interrogation signal from the external reader 180 to the

eye-mountable device 110 to request a measurement. By periodically interrogating the eye-mountable device 110 (e.g., by supplying radio frequency radiation 171 to temporarily turn the device on) and storing the sensor results (e.g., via the data storage 183), the external reader 180 can accumulate a set of analyte concentration measurements over time without continuously powering the eye-mountable device 110.

FIG. 2A is a top view of an example eye-mountable electronic device 210 (or ophthalmic electronics platform). FIG. 2B is an aspect view of the example eye-mountable electronic device shown in FIG. 2A. It is noted that relative dimensions in FIGS. 2A and 2B are not necessarily to scale, but have been rendered for purposes of explanation only in describing the arrangement of the example eye-mountable electronic device 210. The eye-mountable device 210 is formed of a polymeric material 220 shaped as a curved disk. The polymeric material 220 can be a substantially transparent material to allow incident light to be transmitted to the eye while the eye-mountable device 210 is mounted to the eye. The polymeric material 220 can be a biocompatible material similar to those employed to form vision correction and/or cosmetic contact lenses in optometry, such as polyethylene terephthalate ("PET"), polymethyl methacrylate ("PMMA"), polyhydroxyethylmethacrylate ("poly-HEMA"), silicone hydrogels, combinations of these, etc. The polymeric material 220 can be formed with one side having a concave surface 226 suitable to fit over a corneal surface of an eye. The opposite side of the disk can have a convex surface 224 that does not interfere with eyelid motion while the eye-mountable device 210 is mounted to the eye. A circular outer side edge 228 connects the concave surface 224 and convex surface 226.

The eye-mountable device 210 can have dimensions similar to a vision correction and/or cosmetic contact lenses, such as a diameter of approximately 1 centimeter, and a thickness of about 0.1 to about 0.5 millimeters. However, the diameter and thickness values are provided for explanatory purposes only. In some embodiments, the dimensions of the eye-mountable device 210 can be selected according to the size and/or shape of the corneal surface of the wearer's eye.

The polymeric material 220 can be formed with a curved shape in a variety of ways. For example, techniques similar to those employed to form vision-correction contact lenses, such as heat molding, injection molding, spin casting, etc. can be employed to form the polymeric material 220. While the eye-mountable device 210 is mounted in an eye, the convex surface 224 faces outward to the ambient environment while the concave surface 226 faces inward, toward the corneal surface. The convex surface 224 can therefore be considered an outer, top surface of the eye-mountable device 210 whereas the concave surface 226 can be considered an inner, bottom surface. The "bottom" view shown in FIG. 2A is facing the concave surface 226. From the bottom view shown in FIG. 2A, the outer periphery 222, near the outer circumference of the curved disk is curved to extend out of the page, whereas the central region 221, near the center of the disk is curved to extend into the page.

A substrate 230 is embedded in the polymeric material 220. The substrate 230 can be embedded to be situated along the outer periphery 222 of the polymeric material 220, away from the central region 221. The substrate 230 does not interfere with vision because it is too close to the eye to be in focus and is positioned away from the central region 221 where incident light is transmitted to the eye-sensing por-

tions of the eye. Moreover, the substrate **230** can be formed of a transparent material to further mitigate effects on visual perception.

The substrate **230** can be shaped as a flat, circular ring (e.g., a disk with a centered hole). The flat surface of the substrate **230** (e.g., along the radial width) is a platform for mounting electronics such as chips (e.g., via flip-chip mounting) and for patterning conductive materials (e.g., via microfabrication techniques such as photolithography, deposition, plating, etc.) to form electrodes, antenna(e), and/or interconnections. The substrate **230** and the polymeric material **220** can be approximately cylindrically symmetric about a common central axis. The substrate **230** can have, for example, a diameter of about 10 millimeters, a radial width of about 1 millimeter (e.g., an outer radius 1 millimeter greater than an inner radius), and a thickness of about 50 micrometers. However, these dimensions are provided for example purposes only, and in no way limit the present disclosure. The substrate **230** can be implemented in a variety of different form factors, similar to the discussion of the substrate **130** in connection with FIG. **1** above.

A loop antenna **270**, controller **250**, and bio-interactive electronics **260** are disposed on the embedded substrate **230**. The controller **250** can be a chip including logic elements configured to operate the bio-interactive electronics **260** and the loop antenna **270**. The controller **250** is electrically connected to the loop antenna **270** by interconnects **257** also situated on the substrate **230**. Similarly, the controller **250** is electrically connected to the bio-interactive electronics **260** by an interconnect **251**. The interconnects **251**, **257**, the loop antenna **270**, and any conductive electrodes (e.g., for an electrochemical analyte bio-sensor, etc.) can be formed from conductive materials patterned on the substrate **230** by a process for precisely patterning such materials, such as deposition, photolithography, etc. The conductive materials patterned on the substrate **230** can be, for example, gold, platinum, palladium, titanium, carbon, aluminum, copper, silver, silver-chloride, conductors formed from noble materials, metals, combinations of these, etc.

As shown in FIG. **2A**, which is a view facing the convex surface **224** of the eye-mountable device **210**, the bio-interactive electronics module **260** is mounted to a side of the substrate **230** facing the convex surface **224**. Where the bio-interactive electronics module **260** includes an analyte bio-sensor, for example, mounting such a bio-sensor on the substrate **230** to be close to the convex surface **224** allows the bio-sensor to sense analyte concentrations in tear film **42** coating the convex surface **224** of the polymeric material **220** (e.g., a tear film layer distributed by eyelid motion). However, the electronics, electrodes, etc. situated on the substrate **230** can be mounted to either the “inward” facing side (e.g., situated closest to the concave surface **226**) or the “outward” facing side (e.g., situated closest to the convex surface **224**). Moreover, in some embodiments, some electronic components can be mounted on one side of the substrate **230**, while other electronic components are mounted to the opposing side, and connections between the two can be made through conductive materials passing through the substrate **230**.

The loop antenna **270** is a layer of conductive material patterned along the flat surface of the substrate to form a flat conductive ring. In some instances, the loop antenna **270** can be formed without making a complete loop. For instances, the antenna **270** can have a cutout to allow room for the controller **250** and bio-interactive electronics **260**, as illustrated in FIG. **2A**. However, the loop antenna **270** can also be arranged as a continuous strip of conductive material that

wraps entirely around the flat surface of the substrate **230** one or more times. For example, a strip of conductive material with multiple windings can be patterned on the side of the substrate **230** opposite the controller **250** and bio-interactive electronics **260**. Interconnects between the ends of such a wound antenna (e.g., the antenna leads) can then be passed through the substrate **230** to the controller **250**.

FIG. **2C** is a side cross-section view of the example eye-mountable electronic device **210** while mounted to a corneal surface **22** of an eye **10**. FIG. **2D** is a close-in side cross-section view enhanced to show the tear film layers **40**, **42** surrounding the exposed surfaces **224**, **226** of the example eye-mountable device **210**. It is noted that relative dimensions in FIGS. **2C** and **2D** are not necessarily to scale, but have been rendered for purposes of explanation only in describing the arrangement of the example eye-mountable electronic device **210**. For example, the total thickness of the eye-mountable device can be about 200 micrometers, while the thickness of the tear film layers **40**, **42** can each be about 10 micrometers, although this ratio may not be reflected in the figures. Some aspects are exaggerated to allow for illustration and facilitate explanation.

The eye **10** includes a cornea **20** that is covered by bringing the upper eyelid **30** and lower eyelid **32** together over the top of the eye **10**. Incident light is received by the eye **10** through the cornea **20**, where light is optically directed to light sensing elements of the eye **10** (e.g., rods and cones, etc.) to stimulate visual perception. The motion of the eyelids **30**, **32** distributes a tear film across the exposed corneal surface **22** of the eye **10**. The tear film is an aqueous solution secreted by the lacrimal gland to protect and lubricate the eye **10**. When the eye-mountable device **210** is mounted in the eye **10**, the tear film coats both the concave and convex surfaces **224**, **226** with an inner layer **40** (along the concave surface **226**) and an outer layer **42** (along the convex surface **224**). The tear film layers **40**, **42** can be about 10 micrometers in thickness and together account for about 10 microliters.

The tear film layers **40**, **42** are distributed across the corneal surface **22** and/or the convex surface **224** by motion of the eyelids **30**, **32**. For example, the eyelids **30**, **32** raise and lower, respectively, to spread a small volume of tear film across the corneal surface **22** and/or the convex surface **224** of the eye-mountable device **210**. The tear film layer **40** on the corneal surface **22** also facilitates mounting the eye-mountable device **210** by capillary forces between the concave surface **226** and the corneal surface **22**. In some embodiments, the eye-mountable device **210** can also be held over the eye in part by vacuum forces against corneal surface **22** due to the concave curvature of the eye-facing concave surface **226**.

As shown in the cross-sectional views in FIGS. **2C** and **2D**, the substrate **230** can be inclined such that the flat mounting surfaces of the substrate **230** are approximately parallel to the adjacent portion of the convex surface **224**. As described above, the substrate **230** is a flattened ring with an inward-facing surface **232** (closer to the concave surface **226** of the polymeric material **220**) and an outward-facing surface **234** (closer to the convex surface **224**). The substrate **230** can have electronic components and/or patterned conductive materials mounted to either or both mounting surfaces **232**, **234**. As shown in FIG. **2D**, the sensor electronics **260**, controller **250**, and conductive interconnect **251** are mounted on the outward-facing surface **234** such that the sensor electronics **260** are relatively closer in proximity to the convex surface **224** than if they were mounted on the inward-facing surface **232**.

III. Example Ophthalmic Electrochemical Analyte Sensor

FIG. 3 is a functional block diagram of a system 300 for electrochemically measuring a tear film analyte concentration. The system 300 includes an eye-mountable device 310 with embedded electronic components powered by an external reader 340. The eye-mountable device 310 includes an antenna 312 for capturing radio frequency radiation 341 from the external reader 340. The eye-mountable device 310 includes a rectifier 314, an energy storage 316, and regulator 318 for generating power supply voltages 330, 332 to operate the embedded electronics. The eye-mountable device 310 includes an electrochemical sensor 320 with a working electrode 322 and a reference electrode 323 driven by a sensor interface 321. The eye-mountable device 310 includes hardware logic 324 for communicating results from the sensor 320 to the external reader 340 by modulating the impedance of the antenna 312. An impedance modulator 325 (shown symbolically as a switch in FIG. 3) can be used to modulate the antenna impedance according to instructions from the hardware logic 324. Similar to the eye-mountable devices 110, 210 discussed above in connection with FIGS. 1 and 2, the eye-mountable device 310 can include a mounting substrate embedded within a polymeric material configured to be mounted to an eye.

The electrochemical sensor 320 can be situated on a mounting surface of such a substrate proximate the surface of the eye (e.g., corresponding to the bio-interactive electronics 260 on the inward-facing side 232 of the substrate 230) to measure analyte concentration in a tear film layer interposed between the eye-mountable device 310 and the eye (e.g., the inner tear film layer 40 between the eye-mountable device 210 and the corneal surface 22). In some embodiments, however, an electrochemical sensor can be situated on a mounting surface of such a substrate distal the surface of the eye (e.g., corresponding to the outward-facing side 234 of the substrate 230) to measure analyte concentration in a tear film layer coating the exposed surface of the eye-mountable device 310 (e.g., the outer tear film layer 42 interposed between the convex surface 224 of the polymeric material 210 and the atmosphere and/or closed eyelids).

With reference to FIG. 3, the electrochemical sensor 320 measures analyte concentration by applying a voltage between the electrodes 322, 323 that is sufficient to cause products of the analyte catalyzed by the reagent to electrochemically react (e.g., a reduction and/or oxidization reaction) at the working electrode 322. The electrochemical reactions at the working electrode 322 generate an amperometric current that can be measured at the working electrode 322. The sensor interface 321 can, for example, apply a reduction voltage between the working electrode 322 and the reference electrode 323 to reduce products from the reagent-catalyzed analyte at the working electrode 322. Additionally or alternatively, the sensor interface 321 can apply an oxidization voltage between the working electrode 322 and the reference electrode 323 to oxidize the products from the reagent-catalyzed analyte at the working electrode 322. The sensor interface 321 measures the amperometric current and provides an output to the hardware logic 324. The sensor interface 321 can include, for example, a potentiostat connected to both electrodes 322, 323 to simultaneously apply a voltage between the working electrode 322 and the reference electrode 323 and measure the resulting amperometric current through the working electrode 322.

The rectifier 314, energy storage 316, and voltage regulator 318 operate to harvest energy from received radio frequency radiation 341. The radio frequency radiation 341 causes radio frequency electrical signals on leads of the

antenna 312. The rectifier 314 is connected to the antenna leads and converts the radio frequency electrical signals to a DC voltage. The energy storage 316 (e.g., capacitor) is connected across the output of the rectifier 314 to filter out high frequency components of the DC voltage. The regulator 318 receives the filtered DC voltage and outputs both a digital supply voltage 330 to operate the hardware logic 324 and an analog supply voltage 332 to operate the electrochemical sensor 320. For example, the analog supply voltage can be a voltage used by the sensor interface 321 to apply a voltage between the sensor electrodes 322, 323 to generate an amperometric current. The digital supply voltage 330 can be a voltage suitable for driving digital logic circuitry, such as approximately 1.2 volts, approximately 3 volts, etc. Reception of the radio frequency radiation 341 from the external reader 340 (or another source, such as ambient radiation, etc.) causes the supply voltages 330, 332 to be supplied to the sensor 320 and hardware logic 324. While powered, the sensor 320 and hardware logic 324 are configured to generate and measure an amperometric current and communicate the results.

The sensor results can be communicated back to the external reader 340 via backscatter radiation 343 from the antenna 312. The hardware logic 324 receives the output current from the electrochemical sensor 320 and modulates (325) the impedance of the antenna 312 in accordance with the amperometric current measured by the sensor 320. The antenna impedance and/or change in antenna impedance is detected by the external reader 340 via the backscatter signal 343. The external reader 340 can include an antenna front end 342 and logic components 344 to decode the information indicated by the backscatter signal 343 and provide digital inputs to a processing system 346. The external reader 340 associates the backscatter signal 343 with the sensor result (e.g., via the processing system 346 according to a pre-programmed relationship associating impedance of the antenna 312 with output from the sensor 320). The processing system 346 can then store the indicated sensor results (e.g., tear film analyte concentration values) in a local memory and/or an external memory (e.g., by communicating with the external memory through a network).

In some embodiments, one or more of the features shown as separate functional blocks can be implemented ("packaged") on a single chip. For example, the eye-mountable device 310 can be implemented with the rectifier 314, energy storage 316, voltage regulator 318, sensor interface 321, and the hardware logic 324 packaged together in a single chip or controller module. Such a controller can have interconnects ("leads") connected to the loop antenna 312 and the sensor electrodes 322, 323. Such a controller operates to harvest energy received at the loop antenna 312, apply a voltage between the electrodes 322, 323 sufficient to develop an amperometric current, measure the amperometric current, and indicate the measured current via the antenna 312 (e.g., through the backscatter radiation 343).

FIG. 4A is a flowchart of a process 400 for operating an amperometric sensor in an eye-mountable device to measure a tear film analyte concentration. Radio frequency radiation is received at an antenna in an eye-mountable device including an embedded electrochemical sensor (402). Electrical signals due to the received radiation are rectified and regulated to power the electrochemical sensor and associated controller (404). For example, a rectifier and/or regulator can be connected to the antenna leads to output a DC supply voltage for powering the electrochemical sensor and/or controller. A voltage sufficient to cause electrochemical reactions at the working electrode is applied between a

working electrode and a reference electrode on the electrochemical sensor (406). An amperometric current is measured through the working electrode (408). For example, a potentiostat can apply a voltage between the working and reference electrodes while measuring the resulting amperometric current through the working electrode. The measured amperometric current is wirelessly indicated with the antenna (410). For example, backscatter radiation can be manipulated to indicate the sensor result by modulating the antenna impedance.

FIG. 4B is a flowchart of a process 420 for operating an external reader to interrogate an amperometric sensor in an eye-mountable device to measure a tear film analyte concentration. Radio frequency radiation is transmitted to an electrochemical sensor mounted in an eye from the external reader (422). The transmitted radiation is sufficient to power the electrochemical sensor with energy from the radiation for long enough to perform a measurement and communicate the results (422). For example, the radio frequency radiation used to power the electrochemical sensor can be similar to the radiation 341 transmitted from the external reader 340 to the eye-mountable device 310 described in connection with FIG. 3 above. The external reader then receives backscatter radiation indicating the measurement by the electrochemical analyte sensor (424). For example, the backscatter radiation can be similar to the backscatter signals 343 sent from the eye-mountable device 310 to the external reader 340 described in connection with FIG. 3 above. The backscatter radiation received at the external reader is then associated with a tear film analyte concentration (426). In some cases, the analyte concentration values can be stored in the external reader memory (e.g., in the processing system 346) and/or a network-connected data storage.

For example, the sensor result (e.g., the measured amperometric current) can be encoded in the backscatter radiation by modulating the impedance of the backscattering antenna. The external reader can detect the antenna impedance and/or change in antenna impedance based on a frequency, amplitude, and/or phase shift in the backscatter radiation. The sensor result can then be extracted by associating the impedance value with the sensor result by reversing the encoding routine employed within the eye-mountable device. Thus, the reader can map a detected antenna impedance value to an amperometric current value. The amperometric current value is approximately proportionate to the tear film analyte concentration with a sensitivity (e.g., scaling factor) relating the amperometric current and the associated tear film analyte concentration. The sensitivity value can be determined in part according to empirically derived calibration factors, for example.

IV. Example Eye-Mountable Device Identification

FIG. 5A is a block diagram of a system 500 with an eye-mountable device 530 in communication with an external reader 510. The eye-mountable device 530 is configured to be contact-mounted over a corneal surface of an eye 10. The eye-mountable device 530 can operate to output an identification sequence and communicate the identification sequence to the external reader 510. Using the identification sequence, the reader 510 can then retrieve and/or store data specific to the particular device 530, such as configuration and/or calibration information. The reader 510 can differentiate between different eye-mountable devices, using the identification sequences from each, and associate device-specific data with each device. As such, the eye-mountable device 510 does not have any need for on-board programmable memory to store data. Instead, the reader 510 (or a

database accessible by the reader 510) can store device-specific information in a manner that associates the stored information with the identification sequences of the eye-mountable device.

The external reader 510 includes a processing system 512 and a memory 514. The memory 514 can be a volatile and/or non-volatile computer readable media located in the reader 510 and/or in network communication with the reader 510. The memory 514 can be similar to, for example, the memory 182 in the external reader 180 discussed in connection with FIG. 1 above. The processing system 512 can be a computing system that executes software stored in the memory 514 to cause the system 500 to operate as described herein. The reader 510 may be incorporated into a wearable device, such as a device configured to be worn relatively near a user's eye, such as a hat, a headband, an earring, a pendant, eye glasses, etc. The reader 510 may also be incorporated into a watch, a mobile phone, or another personal electronics device.

In some examples, the reader 510 may obtain one or more measurements from sensor(s) on the eye-mountable device 530 (e.g., by intermittently transmitting a measurement signal to cause an electrochemical sensor included in the eye-mountable device 530 to obtain a measurement and communicate the results similar to the system described in connection with FIGS. 1-4). The external reader 510 can also include an antenna (not shown) for transmitting radio frequency radiation 520 to be harvested by the eye-mountable device 530. The external reader 510 can also receive information transmitted back to the reader by backscatter radiation 522. For example, the antenna impedance of the eye-mountable device 530 can be modulated in accordance with an identification sequence such that the backscatter radiation 522 indicates the identification sequence. The backscatter radiation 522 may also indicate sensor measurements, for example. The external reader 510 can also use the memory 514 to store indications of device-specific information 517 (e.g., amperometric current measurements) communicated from the eye-mountable device 530.

FIG. 5B is a block diagram of the eye-mountable device 530 described in connection with FIG. 5A. The eye-mountable device 530 can include energy harvesting systems for harvesting energy from incident radiation 520 (and/or other sources) to power the device 530. For example, electronics for performing measurements and communicating a measurement result can be powered via energy harvesting circuitry.

The eye-mountable device 530 can include communication electronics 532, an identification sequence generator 534, an antenna 536, and a sensor 538 (or other bio-interactive electronics). The identification sequence generator 534 can be configured to output an identification sequence. The identification sequence can be a substantially unique series of values (e.g., a series of binary values) that provide a unique characterizing "fingerprint" for use in distinguishing the particular eye-mountable device 530 from others. The sequence generator 534 can be configured to repeatedly (e.g., consistently) output the series in response to a prompt, such that the same particular device 530 can be consistently associated with the same identification sequence. For example, the identification sequence generator 534 can be a circuit that receives a prompt and outputs the identification sequence. The sequence generator 534 may be a circuit that is incorporated into a control chip of the eye-mountable device 530. In some examples, the identification sequence can be a serial number that is imprinted into the eye-mountable device 530 during a manufacturing pro-

cess. For example, a circuit implementation of the sequence generator **534** can be customized, during manufacture, to output a substantially unique series of high/low values. Each ophthalmic device that is produced can then be assigned a different identification sequence, and the sequence generator circuits of each can be customized accordingly.

Additionally or alternatively, the sequence generator **534** can be configured to generate the identification sequence for the eye-mountable device **530** based on process variations in one or more circuit components. For example, a comparator circuit can be created that compares threshold voltages of two different transistors (or sets of transistors). The uncorrelated threshold voltage variations in such pairs can be amplified and digitized to create a sequence of binary values depending on the state of each comparator circuit. The individual binary state comparator circuits can each be formed from a comparator circuit (e.g., a latch circuit) with cross-coupled logic gates. Following a reset, each comparator circuit settles on one of two possible states depending on the random offset between the threshold voltages. Positive feedback in the cross-coupled arrangement amplifies the small variations to allow for readout. An array of many such circuits can then be used to create an identification sequence with a desired number of bits. Because the resulting identification sequence is based on random, uncorrelated variations in transistor threshold voltage (or other process variations in the die, etc.), the identification sequence may not be entirely unique (i.e., two different identification circuits may generate identical identification sequences). Moreover, such a sequence generator **534** that relies on random process variations may not consistently settle on the same output sequence. For example, comparisons between particularly close threshold voltages may not consistently settle on the same value, and some circuits may systematically change their output over time due to differential degradation of the compared circuit components. However, the probability of such ambiguities can be mitigated by using identification sequences with relatively greater word length (i.e., greater number of bits).

In an example, the sequence generator **534** can include multiple state circuits that are each configured to settle in one of multiple possible states, and each state circuit can then represent a bit (or multiple bits) in the substantially unique identification sequence. An example of such a state circuit can include a cross-coupled NOR gate. A pair of transistors can be arranged to cause the circuit to settle in one state or another depending on the difference in threshold voltage between the two. Each transistor has a gate terminal, a source terminal, and a drain terminal. The conductivity between the drain and source terminals is determined in part by the voltage applied across the gate and source terminals, with a gate-source voltage V_{gs} exceeding a threshold V_{th} resulting in a non-zero drain-source current I_{ds} . The pair of transistors can be connected with the gate of the first transistor connected to the source of the second transistor and the gate of the second transistor connected to the source of the first transistor. The drain of each transistor can be connected to a supply line (e.g., Vdd) and the source of each transistor can be connected to a ground line. The respective connections to the supply line and the ground line can each be made through a transistor driven by a reset line. Upon resetting the circuit the source terminals and cross-coupled gate terminals are all set low (e.g., set to ground).

During the reset to low voltage one of the two cross-coupled transistors becomes conductive before the other one (e.g., the one with the lower threshold voltage). Current through the transistor that becomes conductive first creates

positive feedback to increase the gate-source voltage of the first conductive transistor while decreasing the conductivity of the second transistor, via the cross-coupled drain/gate connection. The drains of the two cross-coupled transistors then settle with one at a high voltage and one at a low voltage, depending on which of the two transistors has a higher threshold voltage. Because the threshold voltage V_{th} is a function of variations in the physical properties of the transistor channel regions (e.g., charge carrier mobility, channel width and length, oxide conductance, etc.), either of the two states occur with roughly equal probability in a given cell due to uncorrelated process variations in the manufacture of the circuit. The drains of the two transistors (or one of them) thus represents an output state of the example state circuit that settles in one of multiple possible states based on random process variations in the manufacture of the state circuit. Other state circuits based on process variations in physical features in the constructed circuitry can also be employed; the above state circuit is described for example purposes only.

Upon receipt of an interrogation signal from the reader **510** (e.g., the radiation **520**), the eye-mountable device **530** can power on (via harvested energy) and the sequence generator **534** can output the identification sequence. The communication electronics **532** can then use the antenna **536** to communicate an indication of the identification sequence back to the reader **510**. For example, the communication electronics **532** may modulate the impedance of the antenna **536** in accordance with the identification sequence, so as to encode information indicative of the identification sequence in the backscatter radiation **522**, which can then be decoded by the reader **510**. The eye-mountable device **530** can also include measurement electronics configured to measure an amperometric current through the working electrode of the sensor **538** and communicate the measured amperometric current through the antenna **536** using the communication electronics **532**.

Upon receipt of the backscatter radiation **522**, the reader **510** can use the identification sequence to access device-specific information **517** in the memory **514**. For example, the reader **510** may lookup configuration and/or calibration data for the device **530**, a date of manufacture, production batch, shipment date, or expiration date of the device **530**, any information regarding prior use of the device **530**, a particular user associated with the device **530**, etc. Such device-specific information **517** may be previously loaded to the memory **514** in connection with manufacture, calibration, testing, or prior use(s) of the device **530**, for example. In addition, the reader **510** may supplement such device-specific information **517** with additional sensor readings, user preferences, etc., such that the additional information is associated with the identification sequence that identifies the particular device **530**. Additionally or alternatively, the reader **510** may access device-specific information stored non-locally (e.g., a database stored on a server in communication with the reader **510**).

Once accessed, the device-specific information **517** can then be used by the reader **510** to operate the eye-mountable device **530**. For example, the reader **510** may use configuration data included in the device-specific information **517** to determine how often (or under what conditions) to query the eye-mountable device **530** for readings. Configuration data may also specify a desired amperometric current stabilization time for the electrochemical sensor **538**, and the reader **510** may therefore be configured to instruct the eye-mountable device **530** to first apply a voltage across electrodes in the sensor **538** for a period while the ampero-

metric current stabilizes (e.g., as the electrochemical reactions at the working electrode reach a steady state). Following the stabilization time, the reader **510** can then prompt the eye-mountable device **530** to measure the amperometric current and indicate the measured current via the backscatter radiation **522**. Other device-specific operation preferences are also possible. Additionally or alternatively, the reader **510** may use calibration data to interpret sensor readings (i.e., amperometric current measurements). Such calibration data may include, for example, a sensitivity and/or offset to define a calibration curve that relates current measurements to analyte concentrations. An example of a calibration procedure and resulting calibration values associated therewith is described below in connection with FIGS. 7-8.

By storing device-specific information **517** off of the device, and mapping such information to the device using the substantially unique identification sequence output from the sequence generator **534**, the device **530** does not require on-board programmable memory. As such, the memory-free device **530** does not store any user-specific information (e.g., prior sensor readings, etc.). Such a memory-free configuration thereby alleviates potential privacy concerns because user-specific information is stored on a platform suitable for incorporating data-protection routines, such as credentialed logins, encryption schemes, etc., which platform may be any combination of the reader **510** and/or external servers. Moreover, the memory-free configuration alleviates concerns over losing data stored in the device **530** in the event of losing the device (e.g., due the device **530** detaching from the eye **10**). As such, the memory-free configuration described herein facilitates implementations in which the eye-mountable device **530** may be a disposable product, similar to a disposable contact lens employed in vision correction applications.

FIGS. 6A-6C illustrate various example processes that may be involved in associating device-specific information with a particular eye-mountable device according to an identification sequence output from the eye-mountable device. FIG. 6A is a process performed by a reader to obtain an identification sequence from an eye-mountable device and then retrieving device-specific information. FIG. 6B is a process performed by an eye-mountable device to communicate an identification sequence for the particular eye-mountable device in response to a query from a reader. FIG. 6C is a process performed by a reader to store device-specific information associated with a particular eye-mountable device by associating the information with the identification sequence for the particular device.

FIG. 6A is a flowchart of an example process **600** for retrieving device-specific information based on an identification sequence received from an eye-mountable device. The process **600** includes transmitting an interrogation signal to an eye-mountable device, at block **602**. For example, the reader **510** may transmit the radiation **520** to the device **530**. Upon receiving the interrogation signal, the eye-mountable device sends a response signal indicating of an identification sequence for the eye-mountable device. The device **530** may output the sequence from the generator **534** and modulating the antenna impedance to cause the backscatter radiation **522** to indicate the identifications sequence. The resulting response signal indicating the identification sequence is received, at block **604**. For example, the reader **510** can receive the backscatter radiation **522**, and the identification sequence can be decoded from the received backscatter. The identification sequence can then be used to retrieve device-specific information, at block **606**. For example, the reader **510** can use the identification sequence

to lookup device-specific configuration, calibration, origin, user, and/or prior usage information **517** in the memory **514** or in a database accessible via the reader **510**.

FIG. 6B is a flowchart of an example process **610** for communicating an identification sequence from an eye-mountable device. The process **610** includes receiving an interrogation signal at an eye-mountable device, at block **612**. For example, the eye-mountable device **530** can receive the radiation **520** from the reader **510**, as described in connection with FIG. 5 above. In response to receiving the interrogation signal (**612**), the eye-mountable device can generate an identification sequence, at block **614**. For example, the identification sequence can be output from the sequence generator **534**, which may be a circuit configured to repeatably (e.g., consistently) output a sequence of bits to form the identification sequence. The identification sequence can be substantially unique, such that a particular eye-mountable device can be substantially unambiguously identified using its identification sequence. The identification sequence can be hard-coded into the sequence generator **534**, similar to a serial number, or the identification sequence may be at least partially output according to one or more circuit components that are configured to settle at one of several possible states based on process variations between the components (e.g., uncorrelated variations in transistor threshold voltages, etc.). The eye-mountable device can then use the antenna to wirelessly communicate an indication of the identification sequence, at block **616**. For example, the communication electronics **532** may modulate the impedance of the antenna **536** so as to encode an indication of the identification sequence in the backscatter radiation **522** (e.g., according to modulations in the amplitude, phase, frequency, etc. of the backscatter).

FIG. 6C is a flowchart of an example process **620** for storing device-specific information for an eye-mountable device. The process **620** includes transmitting an interrogation signal to an eye-mountable device, at block **622**, and receiving the resulting response signal indicating the identification sequence is received, at block **624**. Blocks **622** and **624** are similar to blocks **602** and **604** of the process **600** and cause the reader to obtain an identification sequence for the eye-mountable device. The reader can then determine device-specific information for the eye-mountable device, at block **626**. For example, the reader **510** may obtain a sensor measurement from the eye-mountable device **530** and determine a corresponding analyte concentration. In another example, the reader **510** may perform a calibration on the amperometric sensor in the eye-mountable device **530** and determine one or more calibration values based on such calibration. In another example, the reader **510** may determine a user to associate with the particular eye-mountable device **530** (e.g., via inputs to a user interface of the reader **510** or according to predetermined settings, etc.). Other examples of device-specific information may be determined by the reader **510**. Once such device-specific information is determined, the information can be stored in a format that associates the device-specific information with the identification sequence, at block **628**. As such, the device-specific information can be recalled (e.g., accessed) using the identification sequence to lookup the device-specific information for the particular eye-mountable device **510**. The device-specific information can be stored in the memory **514** of the reader **510** (e.g., the device-specific information **517**) and/or in a database accessible to the reader **510** (e.g., in communication via a network).

V. Example Application: Calibration Information

In some examples, device-specific information that can be associated with a particular eye-mountable device using its identification sequence can include calibration information for one or more sensors included on the device (e.g., the biosensor 162 described in connection with FIG. 1). Such sensors may include, for example, electrochemical analyte sensors, temperature sensors, light sensors (e.g., photocells), corneal pressure sensors (and/or strain sensors), acceleration sensors (accelerometers), and other sensors for obtaining measurements. In some examples, an eye-mountable device may be equipped with sensors for monitoring ophthalmic conditions, such as sensors for measuring corneal shape and/or thickness, for example. Such sensors may also be associated with calibration information to correct for systematic and/or random variations in sensor output in order to map measurements obtained by the sensor to physical quantities. FIGS. 7 and 8 describe an example in which an eye-mountable device with an electrochemical analyte sensor is associated with calibration information for the analyte sensor using its identification sequence. However, it is noted that an eye-mountable device may additionally or alternatively have other sensors (e.g., temperature, light, pressure, etc.) and calibration information may be associated with the eye-mountable device using its identification sequence.

FIG. 7A is a block diagram of an example ophthalmic analyte sensor undergoing calibration. The eye-mountable device 730 can be similar to the eye-mountable devices 110, 210, 310, 530 discussed above in connection with FIGS. 1-6 and includes an electrochemical sensor embedded within a polymeric material configured to be contact-mounted to an eye. The electrochemical sensor includes a working electrode and a reference electrode and can be operated to generate an amperometric current indicating the concentration of an analyte of interest (e.g., glucose). A reagent layer is localized near the working electrode to sensitize the electrochemical sensor to the analyte of interest. The eye-mountable device 730 is powered to measure an analyte concentration by harvesting energy from incident radio frequency radiation 720. The eye-mountable device 730 wirelessly communicates the sensor results to an external reader 710 by backscatter radiation 722.

The reader 710 includes a processing system 712 and a memory 714 storing calibration data 717 and sensor results data 718. The calibration data 717 is used to map sensor measurements to analyte concentration levels. The calibration data 717 can include, for example, coefficients in a function relating sensor measurements to analyte concentrations (e.g., slope and intercept values of a linear relationship), a look-up table relating sensor readings to analyte concentration levels, another indication for used to map sensor measurements to analyte concentration levels, etc. The sensor results data 718 can include one or more previous tear film analyte concentration levels measured with the system 700. Additionally or alternatively, the sensor results data 78 can also include raw sensor outputs (e.g., amperometric current values).

The reader 710 may also include a user input device to indicate to the reader 710 that a calibration procedure is being performed. For example, the user input may signal that sensor measurements are being obtained using a solution with a known analyte concentration, and cause the reader 710 to enter a calibration mode. The user input may also be used to indicate to the reader 710 when the calibration is complete, so the reader 710 can return to a measurement mode for interpreting subsequent in-vitro measurements. Such a user input may also indicate the

concentrations of calibration solutions (if applicable) to allow the reader 710 to interpret amperometric sensor measurements obtained during the calibration. A wireless connection or other data communication technique may also be used to alert the reader 710 that a calibration procedure is being performed.

During calibration, the system 700 updates the calibration data 717 stored in the memory 714 in accordance with a calibration-solution sensor reading. The eye-mountable device 730 is exposed to a calibration solution 740 with a known analyte concentration. The eye-mountable device 730 can be exposed to the calibration solution 740 in a manner that allows the embedded electrochemical analyte sensor to sense the analyte concentration of the calibration solution 740. For example, the eye-mountable analyte sensor 730 can be submerged in a vessel filled with the calibration solution 740, a drop of calibration solution can be placed on the exterior of the eye-mountable device (e.g., convex surface) of the eye-mountable device 730, etc.

The reader 710 obtains a calibration measurement from the eye-mountable device 730 by sending a measurement signal (e.g., the radiation 720). The reader 710 interrogates the eye-mountable device 730 to obtain a reading in a manner similar to the process 420 discussed in connection with FIG. 4B above. For example, the reader 710 can radiate radio frequency radiation 720 to power the eye-mountable device 730 while the eye-mountable device applies voltage across sensor electrodes and measures an amperometric current at the working electrode. The reader 710 can then receive backscatter radiation 722 indicating the measurement result.

The calibration-solution sensor result is used to update (and/or create) the calibration data 717 in the memory 714. The calibration data 717 can be updated by determining a functional relationship for mapping sensor measurements to analyte concentrations. Such a functional relationship can be based entirely on the calibration-solution sensor result. The newly determined functional relationship can additionally or alternatively be based on the calibration-solution sensor result in combination with previously measured calibration data points and/or other assumptions or predictions, etc. The stored calibration data 717 can include one or more calibration value(s) indicative of the determined relationship between sensor measurements and analyte concentrations (e.g., slope and intercept of a linear relationship). It is noted that the present disclosure applies to calibrations of relationships other than linear relationships, such as higher-order polynomial functional relationships, a look-up table, etc.

FIG. 7B is a graph showing example amperometric current values for a range of glucose concentrations. The amperometric current values correspond to measurements by an electrochemical sensor configured to sense glucose. The electrochemical sensor includes a working electrode and a reference electrode driven by a controller, such as a potentiostat. For example, a potentiostat can apply a voltage between the electrodes sufficient to induce electrochemical reactions at the working electrode and thereby generate an amperometric current while measuring the amperometric current. Glucose oxidase is localized near the working electrode to sensitize the sensor to glucose. The glucose oxidase catalyzes glucose to create hydrogen peroxide, which is then oxidized at the working electrode to generate the amperometric current. Human tear film glucose concentrations can range from about 0 millimolar to about 1 millimolar (mM). To calibrate the electrochemical glucose sensor current response over the clinically relevant range,

calibration solutions with known glucose concentrations can be prepared between about 0 mM and about 1 mM, and sensor readings can be obtained while the sensor is exposed to each of the calibration solutions, similar to the calibration mode operation of the system **700** described above in connection with FIG. 7A. For example, the external reader **710** can obtain sensor readings by interrogating the eye-mountable device **630** to perform a measurement while the eye-mountable device **730** is exposed to a calibrated solution. The external reader **710** can then wirelessly receive the sensor result similar to the process. Example results from such a procedure are shown as circles in the graph in FIG. 7B and are listed in the table below.

Glucose Concentration [mM]	Measured Current [nA]
0.02	0.60
0.06	1.36
0.10	2.13
0.15	3.12
0.20	4.04
0.30	6.01
0.50	9.74
0.70	13.4
1.00	19.0

The example calibration data shows a substantially linear relationship between glucose concentration and measured current. The trend line included in the graph in FIG. 7B defines a relationship relating sensor current and glucose concentration over the clinically relevant range of about 0 mM to about 1 mM. The trend line relates the measured currents to the calibrated glucose concentrations. The trend line can be used to determine analyte concentration as a function of sensor current, which can then be used to relate subsequent amperometric current measurements to analyte concentrations. For example, while obtaining in-vitro measurements (similar to the arrangement of the system **500** described in connection with FIG. 5A), the external reader **710** can be programmed to map amperometric currents to corresponding analyte concentrations according to a functional relationship dependent on the amperometric current. That is, a functional relationship can be determined from the calibration data of the form:

$$AC=f(I_{\text{meas}}),$$

where AC is the analyte concentration, I_{meas} is the measured amperometric current, and f represents the functional form stored in the external reader **710** as the calibration data **717**. The determined analyte concentration can then be stored in the sensor measurement data **718** of the memory **714**.

In some embodiments, one or more calibration data points (e.g., a measured sensor result for a known analyte concentration) can be used to determine the functional form of a relationship relating measured current and analyte concentration. For example, any two such calibration data points can be used to solve for coefficients in a first-degree polynomial (e.g., a linear function) by fitting a line to the data points. Additional calibration data points can be used to determine a functional relationship based on a higher order polynomial (e.g., a quadratic functional relationship, etc.). Additionally or alternatively, the functional relationship determined by calibration data can be determined according to a minimization technique (e.g., minimization of χ^2 , etc.) where there are a greater number of calibration data points than degrees of freedom in the functional relationship.

Moreover, in some embodiments, a look-up table listing sensor readings and corresponding analyte concentration levels can be used to map sensor readings to analyte concentrations. For example, entries in such a look-up table can be interpolated to associate a tear film sensor reading with an analyte concentration. In some embodiments, a calibration can be performed on one or more of a batch of eye-mountable electrochemical sensors manufactured under similar conditions, and the derived calibrated functional relationship can be loaded to each such sensor in the batch.

The functional form of the relationship relating measured amperometric currents and analyte concentrations can be set according to an empirically derived calibration data set, according behavior of similar devices, and/or according to theoretical predictions. For example, an eye-mountable electrochemical analyte sensor can be calibrated in connection with its manufacturing process by obtaining sensor outputs (e.g., amperometric currents) while the sensor is exposed to one or more solutions with known analyte concentrations. Regardless of the source of such calibration information, one or more calibration values indicating the determined mapping (e.g., functional relationship) can then be stored in a database and/or in the memory **714** in a manner that associates the calibration information **717** with a substantially unique identification sequence of the eye-mountable device **730**.

FIG. 8A is a flowchart of an example process **800** for calibrating an ophthalmic analyte sensor. The process **800** includes transmitting an interrogation signal to an eye-mountable device, at block **802**, and receiving the resulting response signal indicating the identification sequence is received, at block **804**. Blocks **802** and **804** are similar to blocks **602** and **604** of the process **600** and cause the reader to obtain an identification sequence for the eye-mountable device. A calibration routine is then performed, at block **806**. For example, the calibration routine may include exposing the eye-mountable device **730** to the calibration solution **740** with known analyte concentration (or multiple calibration solutions with different analyte concentrations) and obtaining sensor readings while the device **730** is so exposed. The sensor measurements obtained during calibration can then be used to determine a calibration value that relates the sensor measurements to the known analyte concentrations used during the calibration, at block **808**. For example, the calibration value may indicate a functional relationship for mapping amperometric current measurements to analyte concentrations. The calibration routine and determination of suitable calibration values can be similar to the calibration procedure described above in connection with FIG. 7A. The determined calibration value can then be stored in a database so as to be associated with the device's identification sequence, at block **810**.

FIG. 8B is a flowchart of an example process **820** for interpreting a sensor reading using a predetermined calibration value. The process **820** includes transmitting an interrogation signal to an eye-mountable device, at block **822**, and receiving the resulting response signal indicating the identification sequence is received, at block **824**. Blocks **822** and **824** are similar to blocks **602** and **604** of the process **600** and cause the reader to obtain an identification sequence for the eye-mountable device. Upon determining the identification sequence for the sensor equipped eye-mountable device, the reader can query a database to retrieve calibration information associated with the identification sequence, at block **826**. For example, the reader **710** can lookup previously stored calibration value(s) that define a mapping between amperometric sensor measurements and analyte

concentrations (e.g., coefficients in a functional relationship, entries in a lookup table, etc.). The calibration value(s) retrieved in block 826 can be stored in the memory 714 of the reader 710, or in a networked database in communication with the reader 710. An amperometric sensor measurement is obtained from the eye-mountable device, at block 828. For example, the reader 710 can transmit radiation to the sensor-equipped eye-mountable device 730, the eye-mountable can then perform a measurement and modulate backscatter radiation to indicate the measured current, and the reader 710 can receive the indication of the measurement. The reader can then use the calibration value retrieved from the database to determine the tear film analyte concentration corresponding to the sensor measurement, at block 830. For example, the reader 710 can evaluate the measured amperometric current according to a functional relationship defined by the calibration values, so as to map the measurement to an analyte concentration.

The example processes 800 and 820 of FIGS. 8A and 8B allow for a particular sensor-equipped eye-mountable device to undergo a calibration procedure, and the results of the calibration to be used to interpret subsequent measurements with the sensor. Storing the calibration information in a manner that is associated with the particular eye-mountable device's identification sequence allows for the calibration information (e.g., calibration value(s)) for the particular eye-mountable device to be retrieved during a subsequent measurement using the eye-mountable device without storing such information on the eye-mountable device (e.g., on programmable memory). On the contrary, the eye-mountable device may lack any programmable memory. Instead, any device-specific information can be associated with the identification sequence for the eye-mountable device, and then retrieved subsequently using the identification sequence. Because the eye-mountable device is configured to communicate its identification sequence in response to an interrogation signal, the systems described herein allow for a reader to obtain a particular device's identification sequence, and then retrieve any device-specific for the particular device using the identification sequence. While the example systems and processes described herein disclose sensor calibration information as one example of device-specific information, other examples are possible, such as device manufacture information (e.g., production batch identification, production date, shipment date, expiration date, etc.), associated user information (e.g., user identity, user configuration/profile information, such as number or frequency of measurements to perform for the particular user, predetermined alert levels, etc.), and/or device usage history (e.g., historical sensor measurements, time since last usage, time since last calibration, etc.). Other examples of device-specific information are also possible as the examples provided herein are generally included by way of example and not limitation.

Moreover, it is particularly noted that while the electronics platform is described herein by way of example as an eye-mountable device or an ophthalmic device, it is noted that the disclosed systems and techniques for memory-free configurations of electronics platforms can be applied in other contexts as well. For example, contexts in which bio-sensors are operated with low power budgets (e.g., via harvested energy from radiated sources) or are constrained to small form factors (e.g., implantable bio-sensors or other electronics platforms) may employ the systems and processes described herein to associate device-specific information with particular electronics platforms based on a substantially unique identification sequence output from the

electronics platform. In one example, an implantable medical device that includes a bio-sensor may be encapsulated in biocompatible material and implanted within a host. The implantable medical device may include a circuit configured to output a substantially unique identification sequence (e.g., an array of individual state circuits that consistently settle in one of several possible states according to process variations in the construction of the circuit). Reading and/or control devices can communicate with the implantable medical device to determine the identification sequence and then use the identification sequence to access device-specific information for the device. For example, the reader can query a database using the identification sequence and retrieve and/or store device-specific information. The configurations disclosed herein that are free of programmable memory simultaneously can address spatial constraints in small form factor applications, power budget constraints in low power applications, and/or data security concerns for devices capable of gathering private information.

For example, in some embodiments, the electronics platform may include a body-mountable device, such as a tooth-mountable device. In some embodiments, the tooth-mountable device may take the form of or be similar in form to the eye-mountable device 110, the eye-mountable device 310, and/or the eye-mountable device 530. For instance, the tooth-mountable device may include a biocompatible polymeric material or a transparent polymer that is the same or similar to any of the polymeric materials or transparent polymers described herein and a substrate or a structure that is the same or similar to any of the substrates or structures described herein. In such an arrangement, the tooth-mountable device may be configured to detect at least one analyte in a fluid (e.g., saliva) of a user wearing the tooth-mountable device.

Moreover, in some embodiments, a body-mountable device may comprise a skin-mountable device. In some embodiments, the skin-mountable device may take the form of or be similar in form to the eye-mountable device 110, the eye-mountable device 310, and/or the eye-mountable device 530. For instance, the skin-mountable device may include a biocompatible polymeric material or a transparent polymer that is the same or similar to any of the polymeric materials or transparent polymers described herein and a substrate or a structure that is the same or similar to any of the substrates or structures described herein. In such an arrangement, the skin-mountable device may be configured to detect at least one analyte in a fluid (e.g., perspiration, blood, etc.) of a user wearing the skin-mountable device.

Further, some embodiments of the systems and techniques disclosed herein may include privacy controls which may be automatically implemented or controlled by the wearer of the device. For example, where a wearer's collected physiological parameter data and health state data are uploaded to a cloud computing network for trend analysis by a clinician, the data may be treated in one or more ways before it is stored or used, so that personally identifiable information is removed. For example, a user's identity may be treated so that no personally identifiable information can be determined for the user, or a user's geographic location may be generalized where location information is obtained (such as to a city, ZIP code, or state level), so that a particular location of a user cannot be determined.

Additionally or alternatively, wearers of a device may be provided with an opportunity to control whether or how the device collects information about the wearer (e.g., information about a user's medical history, social actions or activities, profession, a user's preferences, or a user's current

location), or to control how such information may be used. Thus, the wearer may have control over how information is collected about him or her and used by a clinician or physician or other user of the data. For example, a wearer may elect that data, such as health state and physiological parameters, collected from his or her device may only be used for generating an individual baseline and recommendations in response to collection and comparison of his or her own data and may not be used in generating a population baseline or for use in population correlation studies.

Moreover, embodiments that involve information related to a person or a device of a person may include privacy controls. Such privacy controls may include, for example, anonymization of device identifiers, transparency regarding collection/use of information, and user controls including functionality that enables a user to modify and/or delete information relating to the user's use of the device.

Further, in situations in which embodiments discussed herein collect personal information about users, or may make use of personal information, the users may be provided with an opportunity to control whether programs or features collect user information (e.g., information about a user's medical history, social network, social actions or activities, profession, a user's preferences, a user's current location, etc.), or to control whether and/or how to receive content from a content server that may be more relevant to the user. In addition, certain data may be treated in one or more ways before it is stored or used, so that personally identifiable information is removed. For example, a user's identity may be treated so that no personally identifiable information can be determined for the user. Thus, the user may have control over how information is collected about the user and/or used by a content server.

FIG. 9 depicts a computer-readable medium configured according to an example embodiment. In example embodiments, the example system can include one or more processors, one or more forms of memory, one or more input devices/interfaces, one or more output devices/interfaces, and machine-readable instructions that when executed by the one or more processors cause the system to carry out the various functions, tasks, capabilities, etc., described above.

As noted above, in some embodiments, the disclosed techniques can be implemented by computer program instructions encoded on a non-transitory computer-readable storage media in a machine-readable format, or on other non-transitory media or articles of manufacture (e.g., the instructions 184 stored on the memory storage 182 of the external reader 180 of the system 100 or instructions stored on the memory 514 of the reader 510 of the system 500). FIG. 9 is a schematic illustrating a conceptual partial view of an example computer program product that includes a computer program for executing a computer process on a computing device, arranged according to at least some embodiments presented herein.

In one embodiment, the example computer program product 900 is provided using a signal bearing medium 902. The signal bearing medium 902 may include one or more programming instructions 904 that, when executed by one or more processors may provide functionality or portions of the functionality described above with respect to FIGS. 1-8. In some examples, the signal bearing medium 902 can be a non-transitory computer-readable medium 906, such as, but not limited to, a hard disk drive, a Compact Disc (CD), a Digital Video Disk (DVD), a digital tape, memory, etc. In some implementations, the signal bearing medium 902 can be a computer recordable medium 908, such as, but not limited to, memory, read/write (R/W) CDs, R/W DVDs, etc.

In some implementations, the signal bearing medium 902 can be a communications medium 910, such as, but not limited to, a digital and/or an analog communication medium (e.g., a fiber optic cable, a waveguide, a wired communications link, a wireless communication link, etc.). Thus, for example, the signal bearing medium 902 can be conveyed by a wireless form of the communications medium 910.

The one or more programming instructions 904 can be, for example, computer executable and/or logic implemented instructions. In some examples, a computing device such as the processor-equipped external reader 180 of FIG. 1 is configured to provide various operations, functions, or actions in response to the programming instructions 904 conveyed to the computing device by one or more of the computer readable medium 906, the computer recordable medium 908, and/or the communications medium 910.

The non-transitory computer readable medium 906 can also be distributed among multiple data storage elements, which could be remotely located from each other. The computing device that executes some or all of the stored instructions could be an external reader, such as the reader 180 illustrated in FIG. 1, or another mobile computing platform, such as a smartphone, tablet device, personal computer, etc. Alternatively, the computing device that executes some or all of the stored instructions could be remotely located computer system, such as a server.

While various aspects and embodiments have been disclosed herein, other aspects and embodiments will be apparent to those skilled in the art. The various aspects and embodiments disclosed herein are for purposes of illustration and are not intended to be limiting, with the true scope being indicated by the following claims.

What is claimed is:

1. An eye-mountable device comprising:

- a transparent polymeric material having a concave surface and a convex surface, wherein the concave surface removably mounts over a corneal surface and the convex surface is compatible with eyelid motion when the concave surface is so mounted;
- a substrate at least partially embedded within the transparent polymeric material;
- an antenna disposed on the substrate;
- at least one sensor;
- a sequence generator that dynamically generates a substantially unique identification sequence, wherein the substantially unique identification sequence is based on process variations in components of the sequence generator; and
- a controller electrically connected to the antenna, wherein the controller: (i) receives an indication of an interrogation signal via the antenna, (ii) responsive to the interrogation signal, outputs the substantially unique identification sequence, (iii) uses the antenna to communicate the substantially unique identification sequence, (iv) responsive to communicating the substantially unique identification sequence, uses the antenna to receive an indication of device-specific information associated with the eye-mountable device, wherein the device-specific information is a response to said communicating of the substantially unique identification sequence and the device-specific information comprises user-specific information for operating the eye-mountable device, and (v) operates the at least one sensor in accordance with the user-specific information.

2. The eye-mountable device according to claim 1, wherein the sequence generator includes one or more state circuits that output one of multiple possible state outputs based on a difference between one or more circuit components in the one or more state circuits, and wherein the substantially unique identification sequence is based at least in part on the outputs of the one or more state circuits.

3. The eye-mountable device according to claim 1, wherein the sequence generator includes one or more comparator circuits that output a binary state value based on a comparison between an output of circuit components in the one or more comparator circuits, and wherein the substantially unique identification sequence is based at least in part on the binary state value.

4. The eye-mountable device according to claim 1, wherein the controller uses the antenna to indicate a measurement obtained based on the operation of the at least one sensor in accordance with the user-specific information.

5. The eye-mountable device according to claim 4, wherein the at least one sensor includes: an electrochemical analyte sensor, a temperature sensor, a light sensor, a pressure sensor, or an acceleration sensor.

6. The eye-mountable device according to claim 1, wherein the at least one sensor includes an electrochemical sensor disposed on the substrate and including: (i) a working electrode, and (ii) a reference electrode adjacent the working electrode, and

wherein the controller: (i) applies a voltage between the working electrode and the reference electrode sufficient to generate an amperometric current related to a concentration of an analyte in a fluid to which the eye-mountable device is exposed, (ii) measures the amperometric current, and (iii) uses the antenna to indicate the measured amperometric current.

7. The eye-mountable device according to claim 1, further comprising: energy-harvesting circuitry that supplies power to operate the eye-mountable device via radiation received at the antenna.

8. The eye-mountable device according to claim 1, wherein the transparent polymeric material is a substantially transparent vision correction lens and is shaped to provide a predetermined vision-correcting optical power.

9. A method comprising: transmitting an interrogation signal for receipt by an antenna of an eye-mountable device, wherein the antenna is disposed on a substrate at least partially embedded within a transparent polymeric material of the eye-mountable device, and wherein the eye-mountable device includes a sensor;

receiving, from the eye-mountable device, a response signal indicative of a substantially unique identification sequence, wherein the substantially unique identification sequence is based on process variations in components of a sequence generator of the eye-mountable device;

associating the eye-mountable device with device-specific information, wherein the device-specific information is a response to the substantially unique identification sequence received from the eye-mountable device and the device-specific information comprises user-specific information for operating the eye-mountable device; and

causing the eye-mountable device to operate the sensor in accordance with the user-specific information.

10. The method according to claim 9, wherein the associating includes querying a database to determine configuration information for the eye-mountable device.

11. The method according to claim 10, wherein the determined configuration information of the database includes calibration information specific to the of the eye-mountable device.

12. The method according to claim 11, wherein the calibration information is based on at least a previously obtained calibration result of the eye-mountable device.

13. The method according to claim 11, wherein the sensor is an electrochemical analyte sensor, the method further comprising:

determining an analyte concentration corresponding to a sensor measurement from the electrochemical analyte sensor based on the calibration information.

14. The method according to claim 9, wherein the associating includes querying a database to identify a particular user of the eye-mountable device.

15. The method according to claim 14, further comprising determining historical usage data for the identified particular user of the eye-mountable device.

16. The method according to claim 9, wherein the sensor is an electrochemical analyte sensor, the method further comprising:

wirelessly communicating with the eye-mountable device to obtain a measurement from the electrochemical analyte sensor included in the eye-mountable device; and

storing data indicative of the measurement in a database such that the stored data is associated with the substantially unique identification sequence.

17. A non-transitory computer readable medium storing instructions that, when executed by one or more processors in a computing device, cause the computing device to perform operations, the operations comprising:

transmitting an interrogation signal for receipt by an antenna of an eye-mountable device, wherein the antenna is disposed on a substrate at least partially embedded within a transparent polymeric material of the eye-mountable device, and wherein the eye-mountable device includes a sensor;

receiving, from the eye-mountable device, a response signal indicative of a substantially unique identification sequence, wherein the substantially unique identification sequence is based on process variations in components of a sequence generator of the eye-mountable device;

associating the eye-mountable device with device-specific information, wherein the device-specific information is a response to the substantially unique identification sequence received from the eye-mountable device and the device-specific information comprises user-specific information for operating the eye-mountable device; and

causing the eye-mountable device to operate the sensor in accordance with the user-specific information.

18. The non-transitory computer readable medium according to claim 17, wherein the associating includes querying a database to determine configuration information for the eye-mountable device.

19. A body-mountable device comprising:

a bio-compatible polymeric material;

a substrate at least partially embedded within the bio-compatible polymeric material;

an antenna disposed on the substrate;

a sensor;

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a sequence generator that dynamically generates a substantially unique identification sequence, wherein the substantially unique identification sequence is based on process variations in components of the sequence generator; and

a controller electrically connected to the antenna, wherein the controller: (i) receives an indication of an interrogation signal via the antenna, (ii) responsive to the interrogation signal, outputs the substantially unique identification sequence, (iii) uses the antenna to communicate the substantially unique identification sequence, (iv) responsive to communicating the substantially unique identification sequence, uses the antenna to receive an indication of device-specific information associated with the body-mountable device, wherein the device-specific information is a response to said communicating of the substantially unique identification sequence and the device-specific information comprises user-specific information for operating the body-mountable device, and (v) operates the sensor in accordance with the user-specific information.

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20. The body-mountable device according to claim 19, wherein the sensor is an electrochemical sensor disposed on the substrate and including: (i) a working electrode, and (ii) a reference electrode adjacent the working electrode, and

wherein the controller: (i) applies a voltage between the working electrode and the reference electrode sufficient to generate an amperometric current related to a concentration of an analyte in a fluid to which the body-mountable device is exposed, (ii) measures the amperometric current, and (iii) uses the antenna to indicate the measured amperometric current.

21. The body-mountable device according to claim 19, wherein the bio-compatible polymeric material mounts to a tooth surface such that the body-mountable device is a tooth-mountable device.

22. The body-mountable device according to claim 19, wherein the bio-compatible polymeric material mounts to a skin surface such that the body-mountable device is a skin-mountable device.

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[标]申请(专利权)人(译)	谷歌公司		
申请(专利权)人(译)	GOOGLE INC.		
当前申请(专利权)人(译)	实实在在的生命科学LLC		
[标]发明人	OTIS BRIAN YEAGER DANIEL NELSON ANDREW		
发明人	OTIS, BRIAN YEAGER, DANIEL NELSON, ANDREW		
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摘要(译)

可眼戴设备包括嵌入聚合物材料中的控制器，该控制器被配置为安装到眼睛表面。控制器电连接到可眼戴设备中包括的天线。控制器被配置为：(i) 经由天线接收询问信号的指示，(ii) 响应于询问信号，输出基本上唯一的识别序列；(iii) 使用天线传送基本上唯一的识别序列。然后，外部读取器可以使用基本上唯一的识别序列，以将可眼戴设备与设备特定信息相关联，而不将这些信息存储在可眼戴设备上。

