



US010188332B2

(12) **United States Patent**
Lo et al.

(10) **Patent No.: US 10,188,332 B2**
(45) **Date of Patent: Jan. 29, 2019**

(54) **METHOD AND SYSTEM FOR SENSING GLUCOSE CONCENTRATION**

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(*) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 0 days.

(21) Appl. No.: **15/862,611**

(22) Filed: **Jan. 4, 2018**

(65) **Prior Publication Data**
US 2018/0228415 A1 Aug. 16, 2018

(30) **Foreign Application Priority Data**
Feb. 16, 2017 (TW) 106105137 A

(51) **Int. Cl.**
G01J 4/00 (2006.01)
A61B 5/1455 (2006.01)
(Continued)

(52) **U.S. Cl.**
CPC **A61B 5/14558** (2013.01); **A61B 3/102** (2013.01); **A61B 5/0066** (2013.01);
(Continued)

(58) **Field of Classification Search**
CPC ... A61B 5/14558; A61B 3/102; A61B 5/0066;
A61B 5/14532
(Continued)

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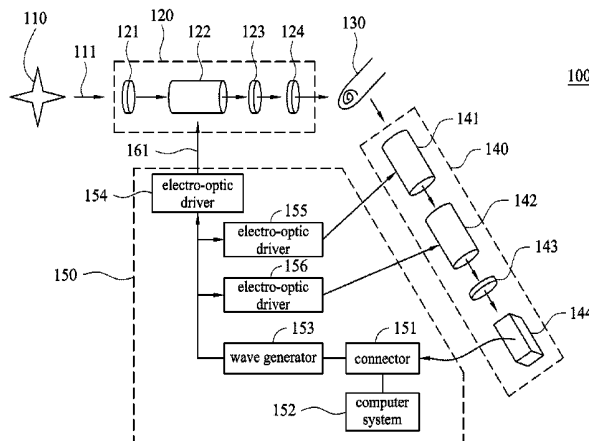
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(57) **ABSTRACT**

A system for sensing glucose concentration is provided and includes following components. A light source generates a light beam. The system may include a polarization state generator (PSG) for changing the polarization of the light beam, and then the light beam is emitted to a biological tissue. A polarization state analyzer (PSA) receives the light beam reflected from the biological tissue, and the received light beam is used to calculate Stokes vectors. A Mueller matrix is calculated according to the Stokes vectors. In some embodiments, the system includes an optical coherence tomography (OCT) in which the light beam is sensed by a detector for calculating the Mueller matrix. An optical rotation angle and a depolarization index are calculated in accordance with the differential Mueller matrix formalism.

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The glucose concentration is calculated in accordance with the optical rotation angle and the depolarization index.

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17 Claims, 8 Drawing Sheets

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A61B 5/145 (2006.01)
A61B 5/00 (2006.01)
G01J 3/447 (2006.01)
A61B 3/10 (2006.01)
- (52) **U.S. Cl.**
CPC *A61B 5/14532* (2013.01); *A61B 5/7235*
(2013.01); *G01J 3/447* (2013.01)
- (58) **Field of Classification Search**
USPC 356/364
See application file for complete search history.

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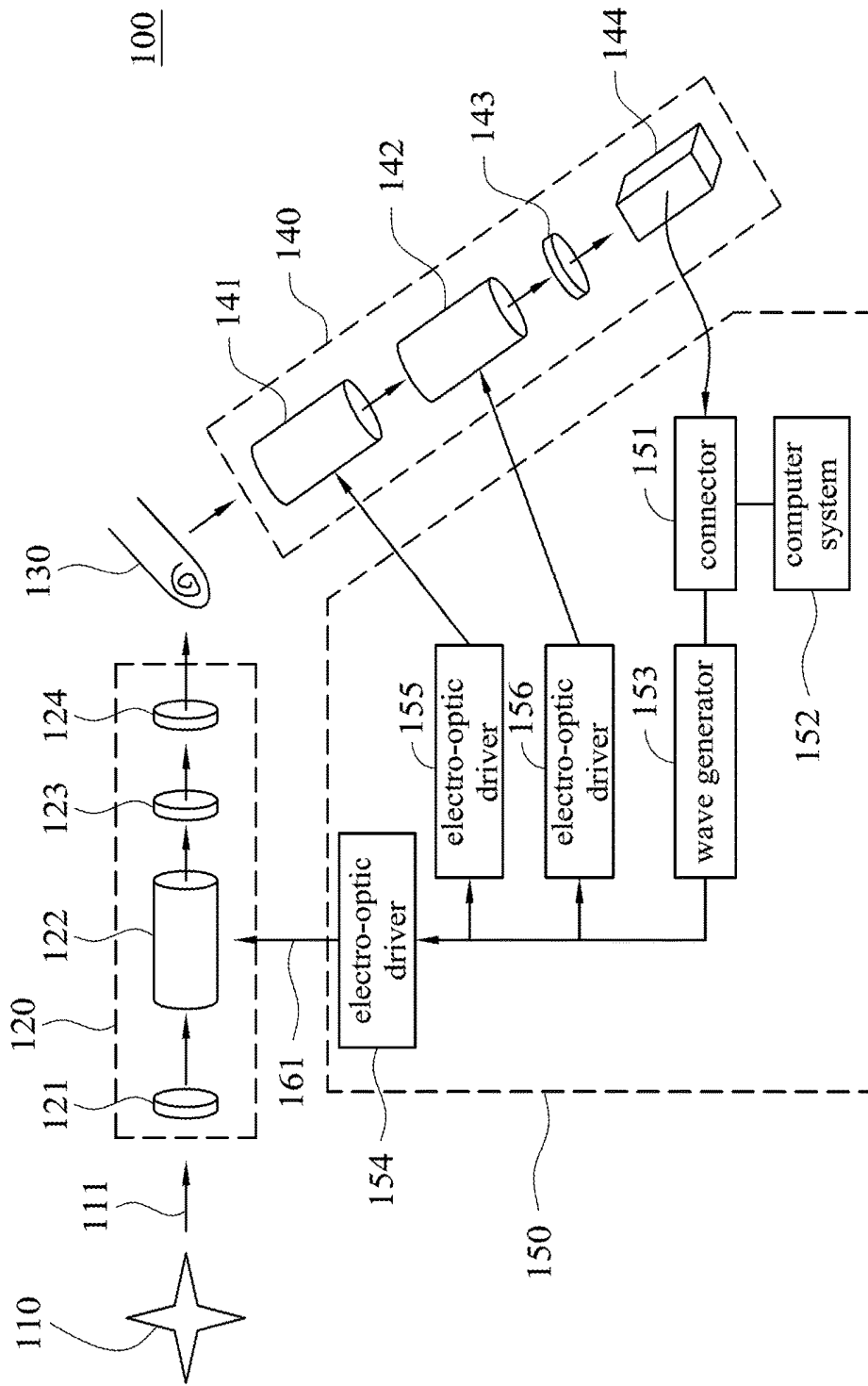


FIG. 1

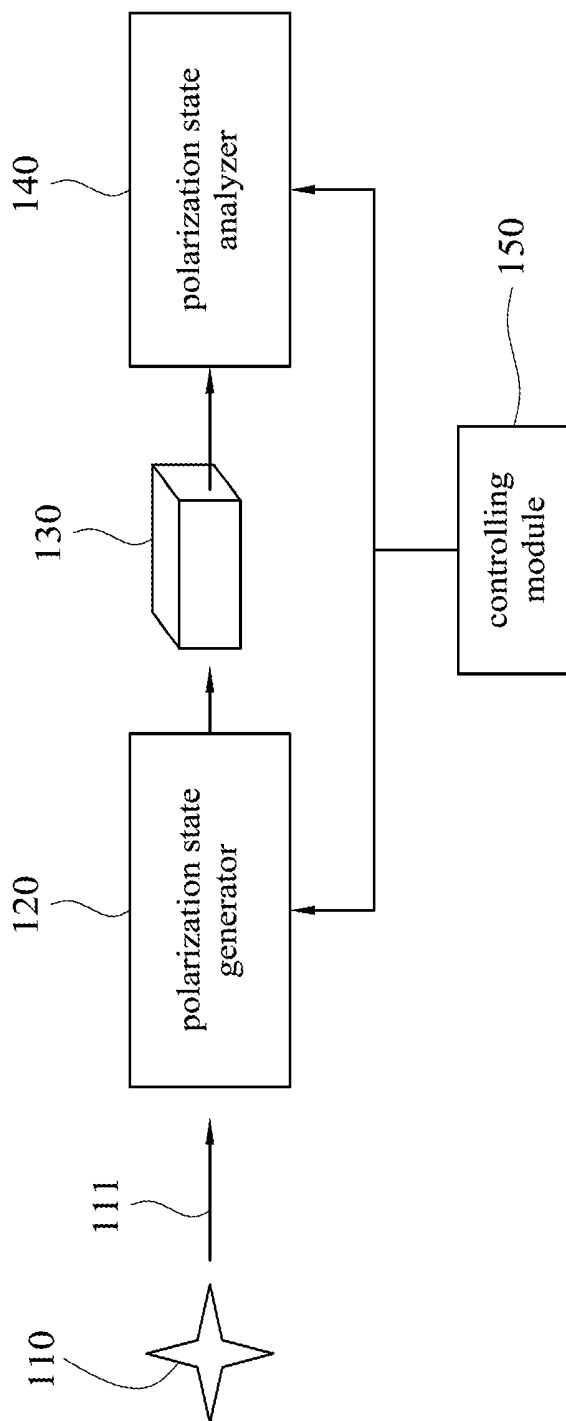


FIG. 2

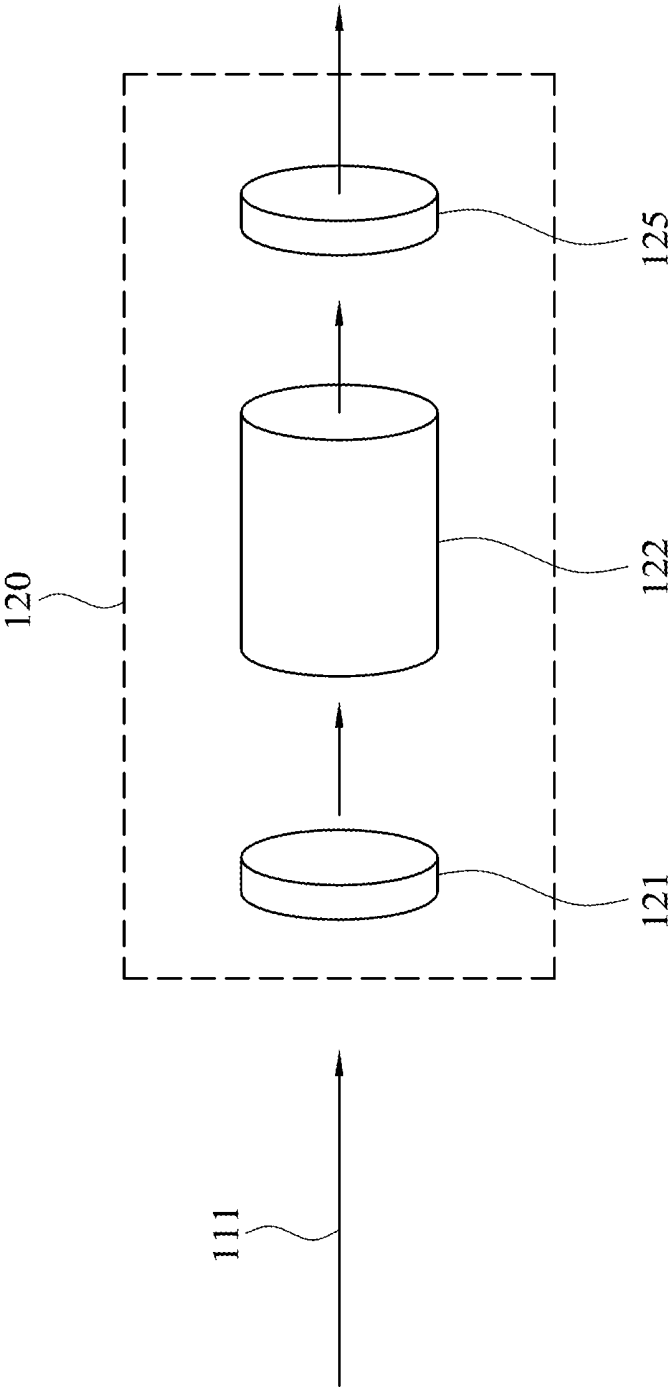


FIG. 3

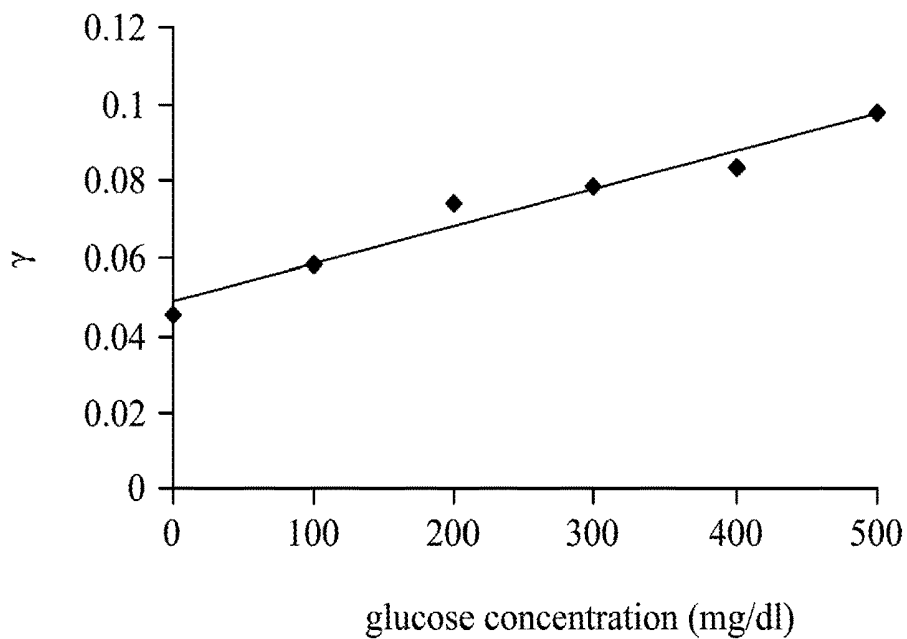


FIG. 4a

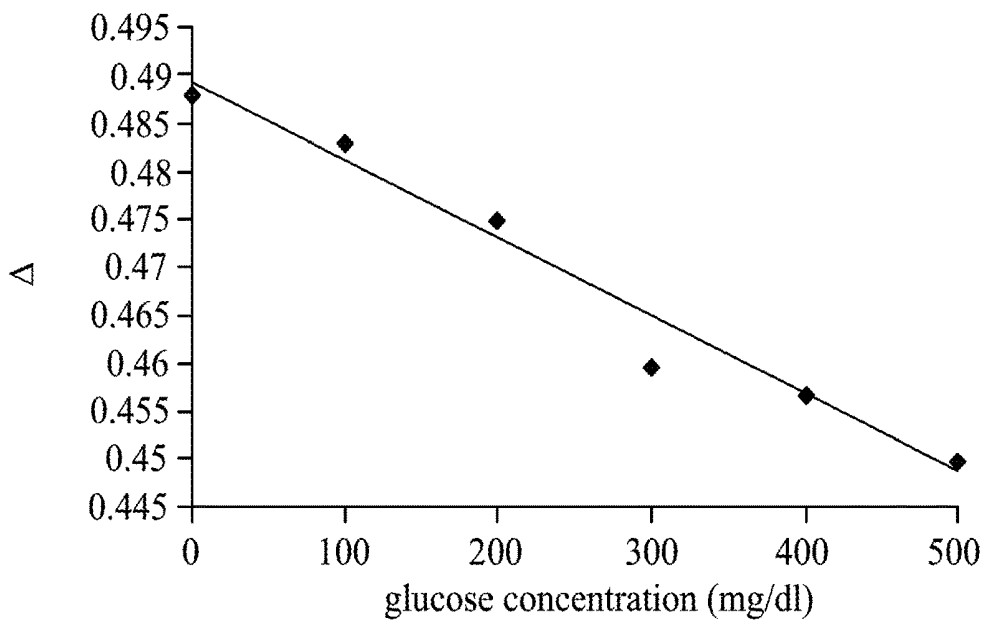


FIG. 4b

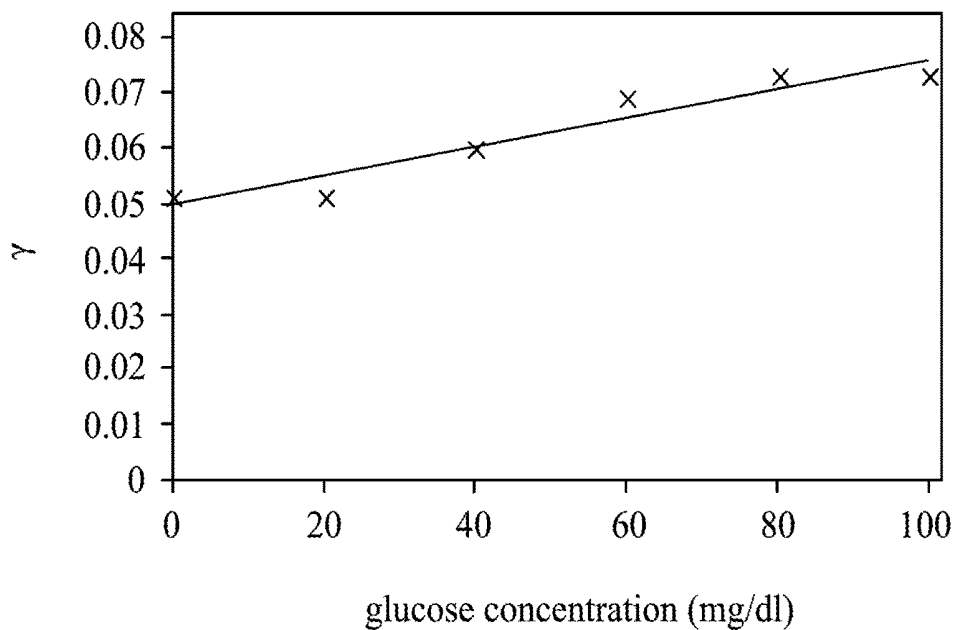


FIG. 5a

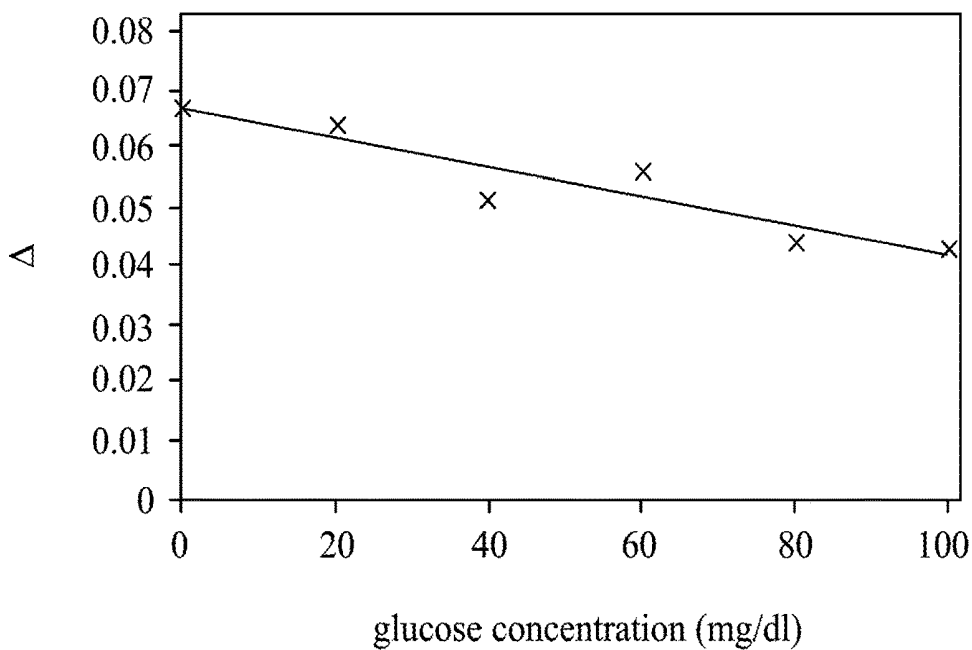


FIG. 5b

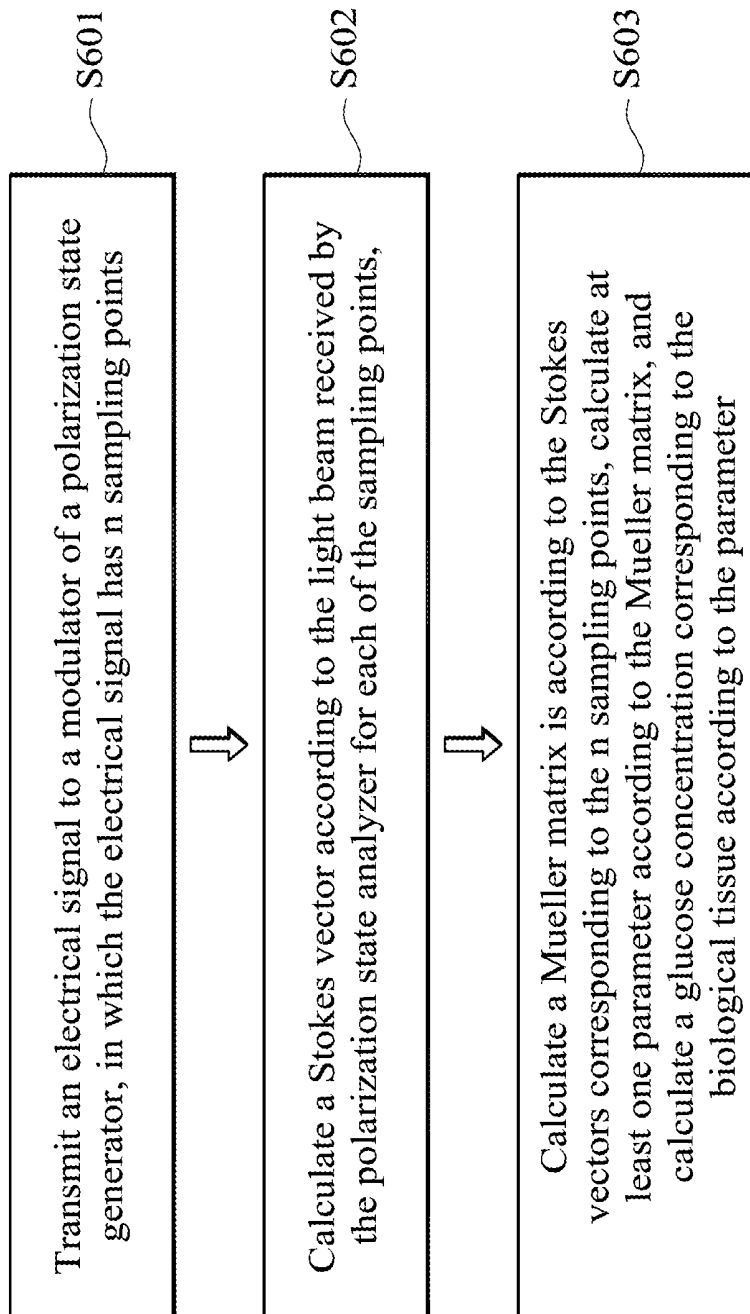


FIG. 6

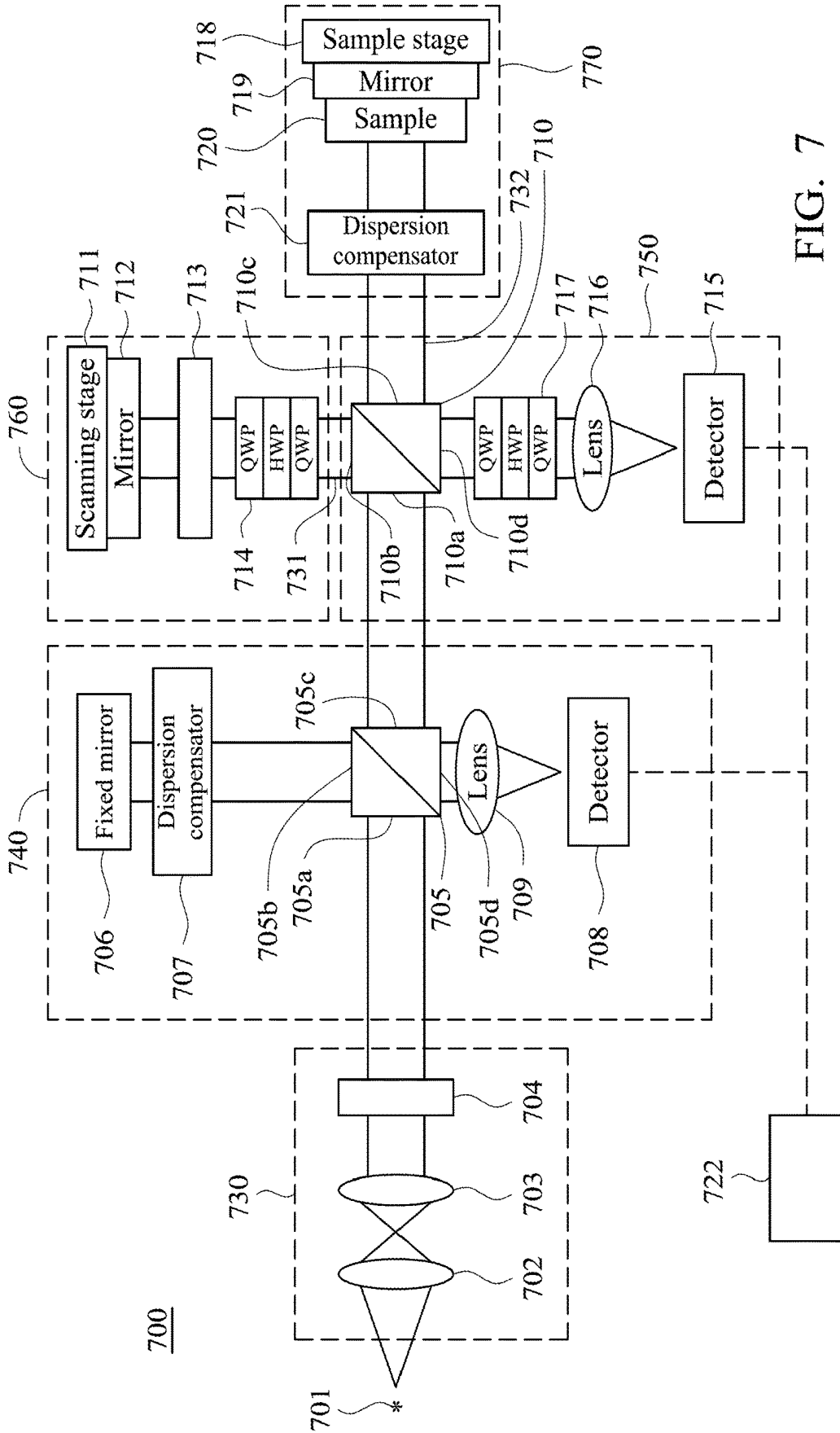


FIG. 7

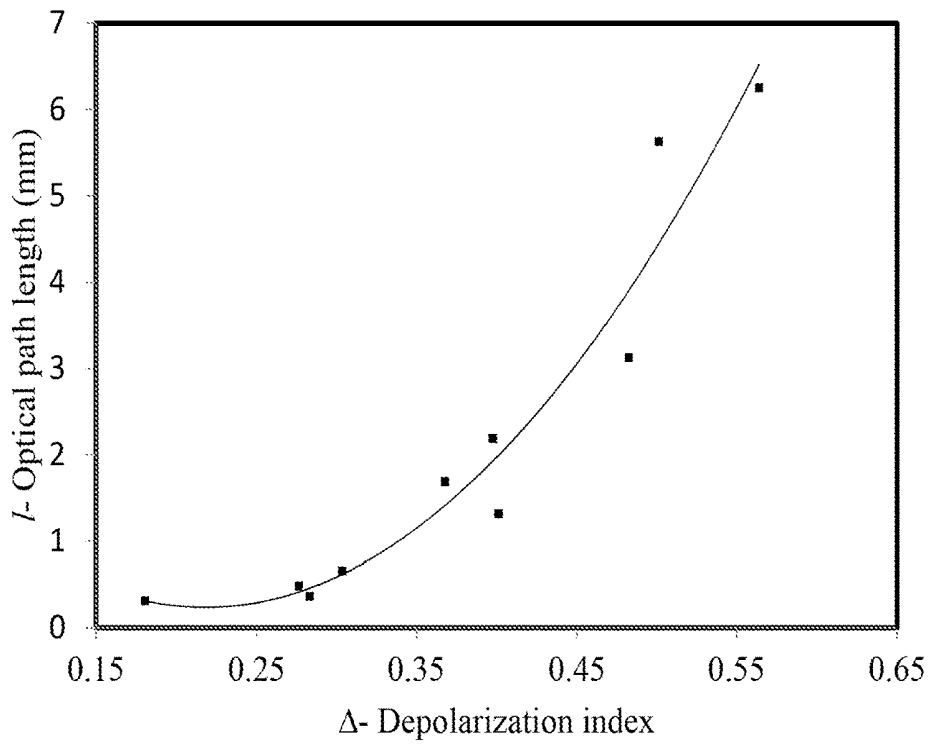


FIG. 8

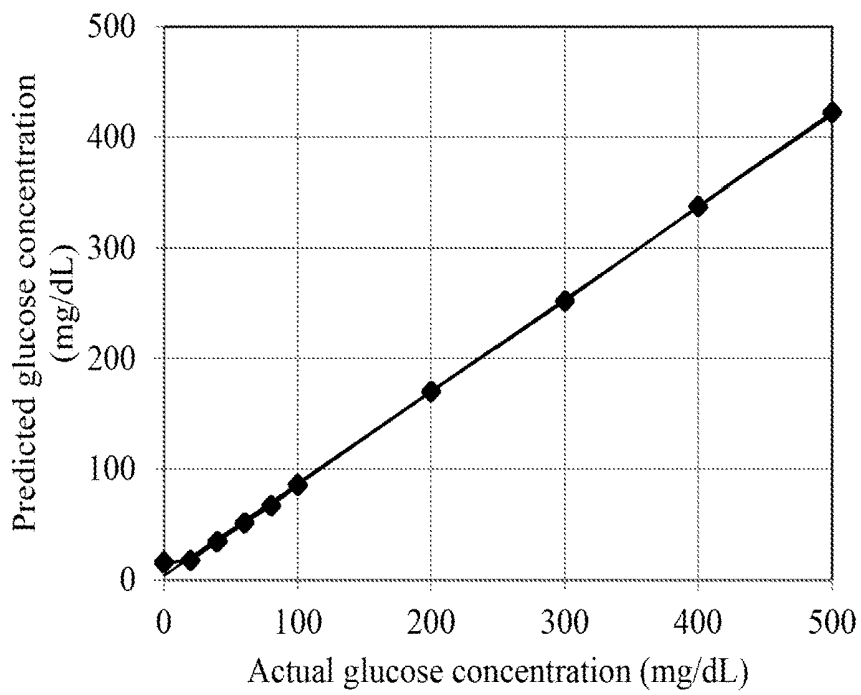


FIG. 9

**METHOD AND SYSTEM FOR SENSING
GLUCOSE CONCENTRATION**

RELATED APPLICATIONS

This application claims priority to Taiwan Application Serial Number 106105137 filed Feb. 16, 2017, which is herein incorporated by reference.

BACKGROUND

Field of Invention

The present invention relates to a non-invasive system for sensing a glucose concentration.

Description of Related Art

A polarization is a basic property of light and has many applications in the industrial or academic fields. In general, the polarization of a light beam can be represented by four Stokes parameters. When the light beam is emitted to an object, the optical property of the object can be represented by a Mueller matrix. Therefore, the mechanism of the Stokes-Mueller matrix can be used to identify many materials or biomaterials. On the other hands, it is an issue in the art about how to measure a glucose concentration of a biological tissue quickly and accurately.

SUMMARY

The system and method provided in the embodiments of the present invention can be applied to a non-invasive measurement and are capable of measuring a low glucose concentration (e.g. 20 mg/dl).

Embodiments of the invention provide a system for sensing glucose concentration. The system includes a light source, a polarization state generator, a polarization state analyzer, and a controlling module. The light source is configured to generate a light beam. The polarization state generator is configured to receive the light beam. The polarization state generator includes a modulator for changing a polarization of the light beam, and the light beam passing the modulator is emitted to a biological tissue. The polarization state analyzer is configured to receive the light beam reflected by the biological tissue. The controlling module is configured to transmit an electrical signal to the modulator. The electrical signal has n sampling points which correspond to n polarizations of the light beam respectively. The n polarizations are different from each other, and n is a positive integer greater than or equal to 4. For each of the n sampling points, the controlling module calculates a Stokes vector according to the light beam received by the polarization state analyzer. The controlling module calculates a Mueller matrix according to the Stokes vectors corresponding to the n sampling points, and calculates at least one parameter according to the Mueller matrix. The at least one parameter includes a depolarization index and an optical rotation angle. The controlling module calculates a glucose concentration corresponding to the biological tissue according to the at least one parameter.

In some embodiments, the polarization state generator further includes a polarizer disposed between the modulator and the light source, and a quarter-wave plate disposed between the modulator and the biological tissue. A principal axis of the polarizer is 0°. A principal axis of the quarter-wave plate is 0°. A principal axis of the modulator is 45°.

In some embodiments, the polarization state generator further includes a polarizer disposed between the modulator and the light source, a quarter-wave plate disposed between the modulator and the biological tissue; and a half-wave plate disposed between the quarter-wave plate and the biological tissue.

In some embodiments, the modulator is an electro-optic modulator. A principal axis of the polarizer is 0°. A principal axis of the electro-optic modulator is 45°. A principal axis of the quarter-wave plate is 45°, and a principal axis of the half-wave plate is 45°. A Stokes vector of the light beam emitted by the polarization state generator is represented by following equations (1) and (2):

$$S' = \begin{bmatrix} 1 \\ \cos a \\ \sin a \\ 1 \end{bmatrix} \quad (1)$$

$$a = \frac{\pi V}{V_{\lambda/2}} \quad (2)$$

S' is the Stokes vector of the light beam emitted by the polarization state generator, V is a constant, and $V_{\lambda/2}$ is an amplitude of the electrical signal.

In some embodiments, the polarization state analyzer includes a second electro-optic modulator with a principal axis of 0°, a third electro-optic modulator with a principal axis of 45°, an analyzer with a principal axis of 0°, and a detector. The second electro-optic modulator is disposed between the biological tissue and the third electro-optic modulator. The analyzer is disposed between the third electro-optic modulator and the detector, and the detector is configured to receive the light beam passing through the second electro-optic modulator, the third electro-optic modulator, and the analyzer.

In some embodiments, the controlling module performs a Fourier transform on brightness of the light beam received by the detector to obtain a plurality of brightness parameters, and calculates a plurality of Stokes parameters of the corresponding Stokes vector according to the plurality of brightness parameters.

In some embodiments, the controlling module calculates a differential Mueller matrix according to following equations (3) and (4).

$$\lambda_m = \ln(\lambda_M)/z \quad (3)$$

$$m = V_M m_\lambda V_M^{-1} = \begin{bmatrix} m_{11} & m_{12} & m_{13} & m_{14} \\ m_{21} & m_{22} & m_{23} & m_{24} \\ m_{31} & m_{32} & m_{33} & m_{34} \\ m_{41} & m_{42} & m_{43} & m_{44} \end{bmatrix} \quad (4)$$

z represents a direction that the light beam propagates along, m is the differential Mueller matrix, V_M represents eigenvectors of the Mueller matrix, λ_M represents eigenvalues of the Mueller matrix, λ_m represents eigenvalues of the differential Mueller matrix, m_λ is a diagonal matrix constituted by the eigenvalues λ_m , and the optical rotation angle is $\gamma = (m_{23} - m_{32})/4$.

In some embodiments, the controlling module generates a differential Mueller matrix m_λ as the following equation (5) according to the differential Mueller matrix m.

$$m_{\Delta} = \begin{pmatrix} 0 & \frac{(m_{12} - m_{21})}{2} & \frac{(m_{13} - m_{31})}{2} & \frac{(m_{14} - m_{41})}{2} \\ \frac{(m_{21} - m_{12})}{2} & m_{22} - m_{11} & \frac{(m_{23} + m_{32})}{2} & \frac{(m_{24} + m_{42})}{2} \\ \frac{(m_{31} - m_{13})}{2} & \frac{(m_{23} + m_{32})}{2} & m_{33} - m_{11} & \frac{(m_{34} + m_{43})}{2} \\ \frac{(m_{41} - m_{14})}{2} & \frac{(m_{24} + m_{42})}{2} & \frac{(m_{34} + m_{43})}{2} & m_{44} - m_{11} \end{pmatrix} \quad (5)$$

The controlling module substitutes the differential Mueller matrix m_{Δ} into the equation (4) to calculate a Mueller matrix M_{Δ} as the following equation (6).

$$M_{\Delta} = \begin{pmatrix} 1 & K_{12} & K_{13} & K_{14} \\ -K_{12} & K_{22} & K_{23} & K_{24} \\ -K_{13} & K_{23} & K_{33} & K_{43} \\ -K_{14} & K_{24} & K_{34} & K_{44} \end{pmatrix} \quad (6)$$

The depolarization index is represented as the following equation (7).

$$\Delta = 1 - \sqrt{\frac{K_{22}^2 + K_{33}^2 + K_{44}^2}{3}} \quad (7)$$

In some embodiments, the controlling module substitutes the parameter γ into a linearly increasing function to obtain the glucose concentration, or substitutes the parameter Δ into a linearly decreasing function to obtain the glucose concentration.

From another aspect, embodiments of the invention provide a method for sensing glucose concentration for a system which includes a light source, a polarization state generator, and a polarization state analyzer. A light beam generated by the light source is emitted to the polarization state generator and then is emitted to a biological tissue, and the polarization state analyzer receives the light beam reflected by the biological tissue. The method includes: transmitting an electrical signal to a modulator of the polarization state generator, in which the electrical signal has n sampling points which correspond to n polarizations of the light beam respectively, the n polarizations are different from each other, and n is a positive integer greater than or equal to 4; calculating a Stokes vector according to the light beam received by the polarization state analyzer for each of the n sampling point; and calculating a Mueller matrix according to the Stokes vectors corresponding to the n sampling points, calculating at least one parameter according to the Mueller matrix, and calculating a glucose concentration corresponding to the biological tissue according to the at least one parameter.

From another aspect, embodiments of the invention provide a system for sensing glucose concentration. The system includes a light source configured to generate a light beam; and an optical coherence tomography (OCT) device for receiving the light beam. The OCT device has at least one detector. A controlling module calculates a Muller matrix according to signals received by the at least one detector, and calculates an optical rotation angle and a depolarization index according to the Muller matrix, and calculates a glucose concentration corresponding to a sample according to the optical rotation angle and the depolarization index.

In some embodiments, the OCT device includes the optical coherence tomography device comprises: a polarization state generator for receiving the light beam and change a polarization of the light beam; a first detecting module for compensating the light beam; a second detecting module coupled to the first detecting module; a reference arm disposed at a side of the second detecting module; and a measurement arm, disposed at another side of the second detecting module.

In some embodiments, the OCT device includes the following components. A polarizer and a quarter-wave plate are configured to receive light. A first non-polarizing beam splitter (NPBS) has a first side, a second side, a third side and a fourth side, in which the first side is opposite to the third side, and the second side is opposite to the fourth side. The polarizer and the quarter-wave plate are disposed at the first side of the first NPBS. A first mirror is disposed at the second side of the first NPBS. A first detector is disposed at the fourth side of the first NPBS. A second NPBS is disposed at the third side of the first NPBS and has a first side, a second side, a third side and a fourth side, in which the first side is opposite to the third side, and the second side is opposite to the fourth side. A second mirror is disposed at the second side of the second NPBS. A variable wave plate is disposed between the second mirror and the second NPBS. A third mirror is disposed at the third side of the second NPBS. The sample is disposed between the third mirror and the second NPBS. A second detector is disposed at the fourth side of the second NPBS.

In some embodiments, the controlling module rotates the quarter-wave plate and the polarizer, and adjusts the variable wave plate to produce at least 16 interferometric signals detected by the second detector. The controlling module calculates the Muller matrix according to the 16 interferometric signals.

In some embodiments, the controlling module obtains an optical path length in accordance with the following equation (8):

$$\Delta = e^{-L/l} \quad (8)$$

where Δ is the depolarization index, L is a length of the sample, and l is the optical path length. The controlling module calculates the glucose concentration corresponding to the sample in accordance with the following equation (9):

$$C = \frac{\gamma}{[\gamma]_T^\lambda} l \quad (9)$$

where C is the glucose concentration, γ is the optical rotation angle, $[\gamma]_T^\lambda$; is the optical rotation angle of the sample at room temperature T, and λ is a wavelength of the light beam.

BRIEF DESCRIPTION OF THE DRAWINGS

The invention can be more fully understood by reading the following detailed description of the embodiment, with reference made to the accompanying drawings as follows.

FIG. 1 is a schematic diagram of a non-invasive system for sensing glucose concentration in accordance with an embodiment.

FIG. 2 is a system for receiving a light beam passing through a biological tissue in accordance with an embodiment.

FIG. 3 is a schematic diagram of a polarization state generator for generating linear polarization in accordance with an embodiment.

FIG. 4a, 4b, 5a, 5b are diagrams illustrating relationships between parameters and the glucose concentration in accordance with an embodiment.

FIG. 6 is a diagram illustrating a flow chart of the method for sensing the glucose concentration in accordance with an embodiment.

FIG. 7 is a schematic diagram illustrating a system for sensing glucose concentration in accordance with some embodiments.

FIG. 8 is a diagram illustrating relationship between the depolarization index and the optical path length.

FIG. 9 is a diagram illustrating relationship between the predicted glucose concentration and the actual glucose concentration.

DETAILED DESCRIPTION

Specific embodiments of the present invention are further described in detail below with reference to the accompanying drawings, however, the embodiments described are not intended to limit the present invention and it is not intended for the description of operation to limit the order of implementation. Moreover, any device with equivalent functions that is produced from a structure formed by a recombination of elements shall fall within the scope of the present invention. Additionally, the drawings are only illustrative and are not drawn to actual size.

The using of “first”, “second”, “third”, etc. in the specification should be understood for identifying units or data described by the same terminology, but are not referred to particular order or sequence.

FIG. 1 is a schematic diagram of a non-invasive system for sensing a glucose concentration in accordance with an embodiment. Referring to FIG. 1, a sensing system 100 includes a light source 110, a polarization state generator (PSG) 120, a polarization state analyzer (PSA) 140 and a controlling module 150. In some embodiments, the sensing system 100 is a portable device, in which one or more components are integrated into a single device, but the shape and the size of the sensing system 100 are not limited in the invention.

The light source 110 emits a light beam 111. The light source 110 is, for example, a laser light source or a broadband light source. The type and the frequency of the light beam 111 are not limited in the invention. In some embodiments, the light source 110 is a He—Ne laser.

The polarization state generator 120 receives the light beam 111, and changes the polarization of the light beam 111. For example, the polarization state generator 120 includes a polarizer 121, an electro-optic modulator (EO) 122, a quarter-wave plate 123 and a half-wave plate 124. In the embodiment, the polarizer 121 is disposed between the light source 110 and the electro-optic modulator 122, the quarter-wave plate 123 is disposed between the electro-optic modulator 122 and the biological tissue 130, and the half-wave plate 124 is disposed between the quarter-wave plate 123 and the biological tissue 130. In other words, after the light beam 111 passes through the polarizer 121, the electro-optic modulator 122, the quarter-wave plate 123 and the half-wave plate 124 sequentially, it is emitted to a biological tissue 130.

In some embodiments, the biological tissue 130 is a human finger. After the light beam is emitted to the biological

tissue, it is reflected to the polarization state generator 140. However, the biological tissue 130 may be any organ or any body part of any animal (including human) in other embodiments. Alternatively, the biological tissue 130 may be blood or other tissues on a carrier or in a container, which is not limited in the invention.

The polarization state analyzer 140 receives the light beam reflected from the biological tissue 130. For example, the polarization state analyzer 140 includes an electro-optic modulator 141 (also referred to as a second electro-optic modulator), an electro-optic modulator 142 (also referred to as a third electro-optic modulator), an analyzer 143 and a detector 144. The electro-optic modulator 141 is disposed between the biological tissue 130 and the electro-optic modulator 142, and the analyzer 143 is disposed between the electro-optic modulator 142 and the detector 144. That is to say, the detector 144 receives the light beam which passes through the electro-optic modulator 141, the electro-optic modulator 142 and the analyzer 143.

The controlling module 150 controls the electro-optic modulators 122, 141, and 142, and receives signals from the detector 144 for calculating a glucose concentration corresponding to the biological tissue 130. In some embodiments, the controlling module 150 includes a connector 151, a computer system 152, a wave generator 153 and electro-optic drivers 154-156. The connector 151 is coupled to the detector 144, the computer system 152 and the wave generator 153. The computer system 152 receives signals from the detector 144 through the connector 151, and transmits instructions/signals to the wave generator 153 through the connector 151. The wave generator 153 controls the electro-optic drivers 154-156 to generate corresponding electrical signals for the electro-optic modulators 122, 141, and 142. However, the invention is not limited thereto, and the controlling module 150 may be implemented as hardware, software, or the combination thereof.

The electro-optic modulators are used to change the polarization of the light beam in the aforementioned embodiments. However, other types of modulators may be used in other embodiments. For example, one or multiple of the electro-optic modulators 122, 141, and 142 may be replaced with magnetic modulators, pressure modulators, or any other suitable type of modulators.

In FIG. 1, the sensing system 100 is non-invasive for sensing the light beam reflected from the biological tissue 130, but the system may sense the light beam passing through the biological tissue 130 in other embodiments. For example, referring to FIG. 2, the components of FIG. 2 that are similar to the components of FIG. 1 are not described again. In FIG. 2, after the light beam 111 passes through the polarization state generator 120, it is emitted to the biological tissue 130 and penetrates the biological tissue 130. The polarization state analyzer 140 would receive the light beam penetrating the biological tissue 130. However, no matter the reflected light beam or the penetrating light beam is sensed, the calculation of glucose concentration described in the following paragraphs would not be affected.

The calculation of the glucose concentration is described herein. Stokes vector and Mueller matrix have to be described first. One Stokes vector has four parameters generally represented as S_0 , S_1 , S_2 , and S_3 . The parameter S_0

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indicates the sum of the power of the electric fields of the light beam (i.e. a type of electromagnetic wave) along two orthogonal directions. The parameter S_1 indicates the difference of the power of the electric fields along the two orthogonal directions. The parameters S_2 , S_3 are used to provide information of the polarization angle and the state of the circular polarization. The person in the art should be able to understand the definition of Stokes vector, and therefore it will not be described in detail.

A general optical sampling is represented as $S_{out} = M \times S_{in}$, where S_{in} is the Stokes vector of the light beam emitted to the biological tissue, and S_{out} is the Stokes vectors of the light beam reflected or penetrating from the biological tissue. The optical properties of the biological tissue can be represented as a Mueller matrix M (also referred to as a macroscopic Mueller matrix) as the following equation (1).

$$S_{out} = \begin{bmatrix} M_{11} & M_{12} & M_{13} & M_{14} \\ M_{21} & M_{22} & M_{23} & M_{24} \\ M_{31} & M_{32} & M_{33} & M_{34} \\ M_{41} & M_{42} & M_{43} & M_{44} \end{bmatrix} \times S_{in} \quad (1)$$

$$m_{BD} = \frac{1}{d} \begin{bmatrix} \ln \left[(1-R^2) \sqrt{\frac{1-D}{1+D}} \right] & -\ln \sqrt{\frac{1-D}{1+D}} \cos(2\theta_d) & -\ln \sqrt{\frac{1-D}{1+D}} \sin(2\theta_d) & \ln \left(\frac{1+R}{1-R} \right) \\ -\ln \sqrt{\frac{1-D}{1+D}} \cos(2\theta_d) & \ln \left[(1-R^2) \sqrt{\frac{1-D}{1+D}} \right] & 2\gamma & -\beta \sin(2\alpha) \\ -\ln \sqrt{\frac{1-D}{1+D}} \sin(2\theta_d) & -2\gamma & \ln \left[(1-R^2) \sqrt{\frac{1-D}{1+D}} \right] & \beta \cos(2\alpha) \\ \ln \left(\frac{1+R}{1-R} \right) & \beta \sin(2\alpha) & -\beta \cos(2\alpha) & \ln \left[(1-R^2) \sqrt{\frac{1-D}{1+D}} \right] \end{bmatrix} \quad (5)$$

The Mueller matrix M may be transformed into one or more differential Mueller matrices to describing different optical properties. It is assumed that the light beam propagates along the z-axis of a right-handed Cartesian coordinate system. The differential Mueller matrix is thus given by the following equation (2).

$$m = (dM/dz)M^{-1} \quad (2)$$

m represents the differential Mueller matrix. The eigenvectors of the Mueller matrix M and the differential Mueller matrix m are represented as V_M and V_m , respectively. The eigenvalues of the Mueller matrix M and the differential Mueller matrix m are represented as λ_M and λ_m , respectively. Assume that the initial condition matrix Mueller matrix $M_{Z=0}$ has the form of an identity matrix. The eigenvalues λ_M and λ_m are related as the following equation (3), and thus the eigenvalues Δ_m can be calculated after the eigenvalues λ_M are obtained.

$$\lambda_m = \ln(\lambda_M)/Z \quad (3)$$

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Assuming that m_λ is a diagonal matrix with diagonal elements of eigenvalues λ_m , the differential Mueller matrix m can be obtained from an eigen analysis of the Mueller matrix M as the following equation (4).

$$m = V_M m_\lambda V_M^{-1} = \begin{bmatrix} m_{11} & m_{12} & m_{13} & m_{14} \\ m_{21} & m_{22} & m_{23} & m_{24} \\ m_{31} & m_{32} & m_{33} & m_{34} \\ m_{41} & m_{42} & m_{43} & m_{44} \end{bmatrix} \quad (4)$$

In accordance with the analysis of the differential Mueller matrix, a general anisotropic sample can be partitioned into 16 different elements, with each element describing a different aspect of the basic optical behavior. Let M_{LB} , M_{CB} , M_{LD} , and M_{CD} be the macroscopic Mueller matrices describing the linear birefringence (LB), circular birefringence (CB), linear dichroism (LD) and circular dichroism (CD) properties. A differential matrix m_{BD} of a composite sample with LB, CB, LD, and CD optical properties can be expressed as the following equation (5).

In the equation (5), d is the sample thickness; α and μ are the orientation angle and phase retardation of the LB property, respectively; γ is the optical rotation angle of the CB property; θ_d and D are the orientation angle and linear dichroism of the LD property, respectively; and R is the circular amplitude anisotropy of the CD property (i.e. $R = (r_R - r_L)/(r_R + r_L)$, $-1 \leq R \leq +1$, where r_R and r_L are the absorptions of right-hand circular polarized light and left-hand circular polarized light, respectively).

The differential Mueller matrix describing the depolarization effect in depolarizing anisotropic media is expressed as the following equation (6).

$$m_\Delta = \frac{1}{d} \begin{bmatrix} 0 & \kappa'_q & \kappa'_u & \kappa'_v \\ -\kappa'_q & -\kappa'_{iq} & \eta'_v & \eta'_u \\ -\kappa'_u & \eta'_v & -\kappa'_{iu} & \eta'_q \\ -\kappa'_v & \eta'_u & \eta'_q & -\kappa'_{iv} \end{bmatrix} \quad (6)$$

The diagonal depolarization is characterized by the parameters K'_{iq} , K'_{iu} , and K'_{iv} . The anomalous dichroism and anomalous depolarization are characterized by the parameters $K'_{q,ii,v}$, and $\eta'_{q,ii,v}$.

The differential Mueller matrix describing all of the LB, CB, LD, CD and Dep properties of an anisotropic optical sample can be obtained by summing equations (5), and (6) as the following equation (7).

$$m_{BD\Delta} = m_{BD} + m_{\Delta} = \frac{1}{d} \begin{pmatrix} \ln\left[(1-R^2)\sqrt{\frac{1-D}{1+D}}\right] & -\ln\sqrt{\frac{1-D}{1+D}} \cos(2\theta_d) + k'_q & -\ln\sqrt{\frac{1-D}{1+D}} \sin(2\theta_d) + k'_u & \ln\left(\frac{1+R}{1-R}\right) + k'_v \\ -\ln\sqrt{\frac{1-D}{1+D}} \cos(2\theta_d) - k'_q & \ln\left[(1-R^2)\sqrt{\frac{1-D}{1+D}}\right] - k'_{iq} & 2\gamma + \eta'_v & -\beta \sin(2\alpha) + \eta'_u \\ -\ln\sqrt{\frac{1-D}{1+D}} \sin(2\theta_d) - k'_u & -2\gamma + \eta'_v & \ln\left[(1-R^2)\sqrt{\frac{1-D}{1+D}}\right] - k'_{iu} & \beta \cos(2\alpha) + \eta'_q \\ \ln\left(\frac{1+R}{1-R}\right) - k'_v & \beta \sin(2\alpha) + \eta'_u & -\beta \cos(2\alpha) + \eta'_q & \ln\left[(1-R^2)\sqrt{\frac{1-D}{1+D}}\right] - k'_{iv} \end{pmatrix} \quad (7)$$

In operation, the macroscopic Mueller matrix M can be determined from the equation (1), and the differential Mueller matrix can be calculated by using the equation (4). The optical parameters describing the anisotropic behavior of the sample can be obtained by equating the differential Mueller matrix of the equation (4) with that of the equation (7). By doing so, the orientation angle α , phase retardation β , optical rotation angle γ , orientation angle θ_d , linear dichroism D and circular dichroism R can be obtained respectively as the following equations (8)-(13).

$$\alpha = \frac{1}{2} \tan^{-1} \left(\frac{m_{42} - m_{24}}{m_{34} - m_{43}} \right) \quad (8)$$

$$\beta = \sqrt{\left[\frac{(m_{42} - m_{24})^2}{2} \right] + \left[\frac{(m_{34} - m_{43})^2}{2} \right]} \quad (9)$$

$$\gamma = \frac{(m_{23} - m_{32})}{4} \quad (10)$$

$$\theta_d = \frac{1}{2} \tan^{-1} \left(\frac{m_{13} + m_{31}}{m_{12} + m_{21}} \right) \quad (11)$$

$$D = \frac{1 - e^{-2\sqrt{(m_{12}+m_{21})^2 + (m_{13}+m_{31})^2}}}{1 + e^{-2\sqrt{(m_{12}+m_{21})^2 + (m_{13}+m_{31})^2}}} \quad (12)$$

$$R = \frac{e^{\frac{(m_{14}+m_{41})}{2}} - 1}{e^{\frac{(m_{14}+m_{41})}{2}} + 1} \quad (13)$$

Similarly, the differential Mueller matrix describing the depolarization effect can be obtained by the following equation (14).

$$m_{\Delta} = \begin{pmatrix} 0 & \frac{(m_{12} - m_{21})}{2} & \frac{(m_{13} - m_{31})}{2} & \frac{(m_{14} - m_{41})}{2} \\ \frac{(m_{21} - m_{12})}{2} & m_{22} - m_{11} & \frac{(m_{23} + m_{32})}{2} & \frac{(m_{24} + m_{42})}{2} \\ \frac{(m_{31} - m_{13})}{2} & \frac{(m_{23} + m_{32})}{2} & m_{33} - m_{11} & \frac{(m_{34} + m_{43})}{2} \\ \frac{(m_{41} - m_{14})}{2} & \frac{(m_{24} + m_{42})}{2} & \frac{(m_{43} + m_{43})}{2} & m_{44} - m_{11} \end{pmatrix} \quad (14)$$

By performing inverse differential calculation on the differential matrix m_{Δ} in accordance with the equation (4), a macroscopic Mueller matrix M_{Δ} is obtained as the following equation (15).

$$M_{\Delta} = \begin{pmatrix} 1 & K_{12} & K_{13} & K_{14} \\ -K_{12} & K_{22} & K_{23} & K_{24} \\ -K_{13} & K_{23} & K_{33} & K_{43} \\ -K_{14} & K_{24} & K_{34} & K_{44} \end{pmatrix} \quad (15)$$

K_{22} and K_{33} are degrees of linear depolarization, and K_{44} is the degree or circular depolarization. In general, the degree of depolarization is quantified by a depolarization index Δ . When the value of the depolarization index Δ is 0, it indicates a non-depolarizing sample; and when the value is 1, it indicates an ideal depolarizer. The depolarization index Δ is expressed as the following equation (16).

$$\Delta = 1 - \sqrt{\frac{K_{22}^2 + K_{33}^2 + K_{44}^2}{3}} \quad (16)$$

Referring to FIG. 1, the calculation of the Mueller matrix is described herein. In some embodiments, the principal axis of the polarizer **121** is 0° , the principal axis of the electro-optic modulator **122** is 45° , the principal axis of the quarter-wave plate **123** is 45° , and the principal axis of the half-wave plate **124** is 45° . In addition, the light beam emitted by the light source **110** is represented as the Stokes vector S_{in} , the light beam emitted by the polarization state generator **120** is represented as the Stokes vector S' , and the relationship between these two vectors are expressed as the following equation (17).

$$S' = H(45^\circ)Q(45^\circ)EO(45^\circ)P(0^\circ)S_{in} \quad (17)$$

The equation (17) can be further expressed as the equation (18).

$$\begin{pmatrix} 1 \\ \cos a \\ \sin a \\ 1 \end{pmatrix} = \begin{pmatrix} 1 & 0 & 0 & 0 \\ 0 & 1 & 0 & 0 \\ 0 & 0 & -1 & 0 \\ 0 & 0 & 0 & -1 \end{pmatrix} \begin{pmatrix} 1 & 0 & 0 & 0 \\ 0 & 1 & 0 & 0 \\ 0 & 0 & 0 & -1 \\ 0 & 0 & 1 & 0 \end{pmatrix} \begin{pmatrix} 1 & 0 & 0 & 0 \\ 0 & \cos a & 0 & -\sin a \\ 0 & 0 & 1 & 0 \\ 0 & \sin a & 0 & \cos a \end{pmatrix} \quad (18)$$

$$\begin{pmatrix} 1/2 & 1/2 & 0 & 0 \\ 1/2 & 1/2 & 0 & 0 \\ 0 & 0 & 0 & -1 \\ 0 & 0 & 1 & 0 \end{pmatrix} \begin{pmatrix} 1 \\ 1 \\ 0 \\ 0 \end{pmatrix}$$

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In the equation (18), a is a parameter for adjusting phase retardation of the electro-optic modulator **122**. The electro-optic driver **154** outputs an electrical signal **161** to the electro-optic modulator **122** for changing the parameter a . To be specific, the parameter a can be expressed as the following equation (19).

$$a = \frac{\pi V}{V_{\lambda/2}} \quad (19)$$

In the equation (19), V is a constant, and $V_{\lambda/2}$ is the amplitude of the electrical signal **161**. In some embodiments, the electrical signal **161** is a periodic saw-tooth signal. However, the invention is not limited thereto, other forms of signals such as sine wave, cosine wave, square wave, or any other wave can be applied in other embodiments. Besides, the electrical signal **161** may be a non-periodic signal in other embodiments.

In the embodiment of FIG. 1, the polarization state generator **120** is used to generate the light beam with circular polarization. However, in other embodiments, the polarization state generator **120** may be used to generate the light beam with linear polarization. For example, referring to FIG. 3, the polarization state generator **120** includes a polarizer **121**, an electro-optic modulator **122** and a quarter-wave plate **125**. The principal axis of the polarizer **121** is 0° , the principal axis of the electro-optic modulator **122** is 45° , and the principal axis of the quarter-wave plate **125** is 45° . In the embodiment of FIG. 3, the relationship between the Stokes vector S_m and the Stokes vector S' is expressed as the following equations (20) and (21).

$$S' = Q(0^\circ)EO(45^\circ)S_m \quad (20)$$

$$\begin{bmatrix} 1 \\ \cos a \\ \sin a \\ 0 \end{bmatrix} = \begin{bmatrix} 1 & 0 & 0 & 0 \\ 0 & 1 & 0 & 0 \\ 0 & 0 & 0 & 1 \\ 0 & 0 & -1 & 0 \end{bmatrix} \begin{bmatrix} 1 & 0 & 0 & 0 \\ 0 & \cos a & 0 & -\sin a \\ 0 & 0 & 1 & 0 \\ 0 & \sin a & 0 & \cos a \end{bmatrix} \begin{bmatrix} 1 \\ 1 \\ 0 \\ 0 \end{bmatrix} \quad (21)$$

Similarly, the electro-optic driver **154** outputs the electrical signal **161** to the electro-optic modulator **122** for changing the parameter a . The electro-optic modulator **122** is used to change the polarization of the light beam no matter circular polarization or the linear polarization is adopted. Since the light beam with a certain polarization has four Stokes parameters, and the Mueller matrix has 16 unknown variables, we need at least four polarizations of the light beam to determine the Mueller matrix. In the embodiment, one period of the electrical signal **161** has n sampling points which correspond to n different parameters a . In other words, the n sampling points correspond to n polarizations which are different from each other. In addition, n is a positive integer greater than or equal to 4. For example, the positive integer n may be equal to 200, which is not limited in the invention. In other embodiments, the positive integer n may be any integer greater than 50, 100 or 300.

The light beam with different polarizations is emitted to the biological tissue **130** and is received, after reflected or penetrating from the biological tissues **130**, by the polarization state analyzer **140**. In some embodiments, the principal axis of the electro-optic modulator **141** is 0° , the principal axis of the electro-optic modulator **142** is 45° , and the principal axis of the analyzer **143** is 0° . Therefore, the Stokes

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vector S_{OUT} of the light beam received by the detector **144** is expressed by the following equation (22).

$$S_{OUT} = A(0^\circ)EO(45^\circ)EO(0^\circ)S' \quad (22)$$

The equation (22) can be further expressed as the following equation (23).

$$\begin{bmatrix} I(\beta_1, \beta_2) \\ I(\beta_1, \beta_2) \\ 0 \\ 0 \end{bmatrix} = \begin{bmatrix} 1/2 & 1/2 & 0 & 0 \\ 1/2 & 1/2 & 0 & 0 \\ 0 & 0 & 0 & 0 \\ 0 & 0 & 0 & 0 \end{bmatrix} \begin{bmatrix} 1 & 0 & 0 & 0 \\ 0 & \cos \beta_2 & 0 & -\sin \beta_2 \\ 0 & 0 & 1 & 0 \\ 0 & \sin \beta_2 & 0 & \cos \beta_2 \end{bmatrix} \begin{bmatrix} S_0 \\ S_1 \\ S_2 \\ S_3 \end{bmatrix} \quad (23)$$

In the equation (23), β_1 and β_2 are parameters for adjusting phase retardation of the electro-optic modulators **141** and **142** respectively and they are controlled in accordance with the equation (19). In other words, the electro-optic drivers **155** and **156** transmit two electrical signals to the electro-optic modulators **141** and **142** respectively, and the amplitudes of these two electrical signals are the parameter $V_{\lambda/2}$ in the equation (19). Accordingly, the brightness of the light beam received by the detector **144** is expressed as the following equation (24).

$$I(\beta_1, \beta_2) = A + B \cos \beta_2 + C \sin \beta_1 \sin \beta_2 + D \cos \beta_1 \sin \beta_2 \quad (24)$$

If the parameters β_1 and β_2 are the same, then the equation (24) is written as the following equation (25).

$$I(\beta_1) = A + B \cos(\beta_1) + C \sin(2\beta_1) + D \sin(2\beta_1) \quad (25)$$

In the equation (25), $A = 0.5 S_0 - 0.25 S_2$, $B = 0.5 S_1$, $C = 0.25 S_2$, and $D = 0.25 S_3$. The controlling module **150** performs a Fourier transform on the light beam received by the detector **144** to obtain the brightness parameters A , B , C , and D , and calculates Stokes parameters of the corresponding Stokes vector based on these brightness parameters. In detail, the brightness parameters A , B , C , and D are obtained as the following equations (26)-(29) respectively.

$$A = \frac{1}{2\pi} \int_{-\beta_{\lambda/2}}^{\beta_{\lambda/2}} I(\beta_1).d(\beta_1) \quad (26)$$

$$B = \frac{1}{\pi} \int_{-\beta_{\lambda/2}}^{\beta_{\lambda/2}} I(\beta_1).\cos(\beta_1).d(\beta_1) \quad (27)$$

$$C = \frac{1}{\pi} \int_{-\beta_{\lambda/2}}^{\beta_{\lambda/2}} I(\beta_1).\cos(2\beta_1).d(\beta_1) \quad (28)$$

$$D = \frac{1}{\pi} \int_{-\beta_{\lambda/2}}^{\beta_{\lambda/2}} I(\beta_1).\sin(2\beta_1).d(\beta_1) \quad (29)$$

$\beta_{\lambda/2}$ is the induced half-wave retardation. Once the brightness parameters A , B , C , and D are known, the Stokes parameters S_0 - S_3 can be obtained.

For each sampling point of the electrical signal, the controlling module calculates the corresponding Stokes vector according to the light beam received by the polarization state analyzer. In the embodiment, there are 200 Stokes vectors in one period. Therefore, the Mueller matrix M can

be obtained in accordance with the equation (1), and the differential Mueller matrix m is calculated in accordance with the equations (3) and (4). After the differential Mueller matrix is obtained, the parameters such as the orientation angle α , the phase retardation β , the optical rotation angle γ , the orientation angle θ_d , the linear dichroism D and the circular amplitude anisotropy R can be obtained in accordance with the equations (8)-(13). In some embodiments, there may not be a set of parameters α , β , γ , θ_d , D , R causing that the equation (4) is perfectly matched with the equation (7). Therefore, some numerical methods may be adopted to find the set of parameters α , β , γ , θ_d , D , R for minimizing the error between the equation (4) and the equation (7). For example, the root mean square error of all elements between the equation (4) and the equation (7) may be set as an objective function, and the parameters α , β , γ , θ_d , D , R serve as a DNA to perform a genetic algorithm. However, how the parameters α , β , γ , θ_d , D , R are found is not limited in the invention. On the other hand, the depolarization index Δ can be obtained in accordance with the equations (14)-(16). In the embodiment, the optical rotation angle γ and the depolarization index Δ are used to calculate the glucose concentration.

To be specific, FIG. 4a, 4b, 5a, 5b are diagrams illustrating relationships between parameters and the glucose concentration in accordance with an embodiment. FIG. 4a shows the relationship between the optical rotation angle γ and the glucose concentration, and the relationship is approximated as a linearly increasing function. FIG. 4b shows the relationship between the depolarization index Δ and the glucose concentration, and the relationship is approximated as a linearly decreasing function. FIG. 5a is similar to FIG. 4a, and FIG. 5b is similar to FIG. 4b, except for the different glucose concentration. Note that the glucose concentration around 20 mg/dl can be measured in FIG. 5a and FIG. 5b.

In some embodiments, the controlling module 150 may substitute the parameter γ into a linearly increasing function to calculate the glucose concentration, or substitute the parameter Δ into a linearly decreasing function to calculate the glucose concentration. The linearly increasing function or the linearly decreasing function may be represented as $y=ax+b$ where y is the glucose concentration, x is the parameter γ or Δ , and a and b are constants. However, the invention is not limited thereto. In other embodiments, the parameter γ , Δ , or the combination thereof may be taken as input, and the known glucose concentration is taken as output for performing a regression analysis to obtain constants in a mathematic model. The mathematic model may be a linear function (applied in the embodiment), a polynomial function, an exponential function, or other functions. Moreover, how many constants exist in the mathematic model is not limited in the invention. For example, if the polynomial function is applied, the model may be expressed as $y=ax^2+bx+c$ where a , b , and c are constants, and x is the parameter γ or Δ . The person in the art should be able to understand the regression analysis and figure out another mathematic model. Alternatively, the parameter γ , Δ , or the combination thereof may be taken as input, the known glucose concentration is taken as output to train a machine learning model such as neural network, support vector machine, etc. In some embodiments, the parameter γ , Δ , or the combination thereof may be just a portion of the input.

In the aforementioned embodiments, the differential Mueller matrix is used to calculate the parameters γ and Δ , but in other embodiments, the parameters γ and Δ may be calculated by decomposing the Mueller matrix, which is not

limited in the invention. For example, another algorithm for calculating the parameters γ and Δ are disclosed by the thesis "Extraction of effective parameters of turbid media utilizing Mueller matrix approach: study of glucose sensing", Journal of Biomedical Optics 17(9), 097002 (2012) written by Thi-Thu-Hien Pham and Yu-Lung Lo and this algorithm may also be applied in the sensing system of the present application. On the other hand, the Stokes vectors are calculated by the polarization state analyzer 140 by using Fourier transform in the aforementioned embodiment, but in other embodiments, the Stokes vector may be calculated by adopting other suitable device and/or algorithms, which is not limited in the invention.

In the embodiments, the glucose concentration can be calculated in one period (e.g. 1/80 k seconds) of the electrical signal. Therefore, the measurement is done very quickly that can avoid external interference and thus increase the measurement accuracy. In some embodiments, one glucose concentration is calculated in each period, and the average of the glucose concentrations in a short time (e.g. one second) is calculated. However, the person in the art should be able to adjust the parameters such as period, time, etc., which is not limited in the invention. Alternatively, some signal processing approaches such as noise removing, extreme value removing may be performed on the obtained glucose concentrations. The content of the signal processing is not limited in the invention.

FIG. 6 is a diagram illustrating a flow chart of the method for sensing the glucose concentration in accordance with an embodiment. The method may be applied to the embodiments of FIG. 1, FIG. 2 or FIG. 3. In step S601, an electrical signal is transmitted to a modulator of a polarization state generator, in which the electrical signal has n sampling points. In step S602, for each of the sampling points, a Stokes vector is calculated according to the light beam received by the polarization state analyzer. In step S603, a Mueller matrix is calculated according to the Stokes vectors corresponding to the n sampling points, at least one parameter is calculated according to the Mueller matrix, and a glucose concentration corresponding to the biological tissue is calculated according to the parameter. However, all the steps in FIG. 6 have been described in detail above, and therefore they will not be repeated. Note that the steps in FIG. 6 can be implemented as program codes or circuits, and the disclosure is not limited thereto. In addition, the method in FIG. 6 can be performed with the aforementioned embodiments, or can be performed independently. In other words, other steps may be inserted between the steps of the FIG. 6.

In the system and method provided in the embodiments of the invention, the glucose concentration as low as 20 mg/dl can be measured. In addition, the sensing system could be noninvasive that only needs to emit the light beam to a human finger, and thus the glucose measurement is very simple and convenient.

FIG. 7 is a schematic diagram illustrating a system 700 for sensing glucose concentration in accordance with some embodiments. Referring to FIG. 7, the system 700 includes a light source 701 and an optical coherence tomography (OCT) device. The light source 701 (e.g. a thermal light source is adopted to enhance the axial resolution) is configured to generate a light beam. The OCT device includes a polarization state generator 730 for receiving the light beam and change the polarization of the light beam; a first detecting module 740 for compensating and splitting the light beam; a second detecting module 750 coupled to the first detecting module for splitting the light beam again; a

reference arm **760** disposed at a side of the second detecting module **750**; a measurement arm **770** disposed at another side of the second detecting module **750**.

In detail, the light beam passes through the lens **702** and **703**, and then is emitted to a combined polarizer and quarter-wave plate **704**. A first non-polarizing beam splitter (NPBS) **705** has a first side **705a**, a second side **705b**, a third side **705c** and a fourth side **705d**. The first side **705a** is opposite to the third side **705c**, and the second side **705b** is opposite to the fourth side **705d**. The polarizer and quarter-wave plate **704** is disposed at the first side **705a** of the first NPBS **705**. A fixed mirror **706** is disposed at the second side **705b**. A dispersion compensator **707** is disposed between the mirror **706** and the first NPBS **705**. A detector **708** is disposed at the fourth side **705d** of the first NPBS **705**. A lens **709** is disposed between the detector **708** and the first NPBS **705**. A second NPBS **710** is disposed at the third side **705c** of the first NPBS **705**. The NPBS **710** has a first side **710a**, a second side **710b**, a third side **710c** and a fourth side **710d**, in which the first side **710a** is opposite to the third side **710c**, and the second side **710b** is opposite to the fourth side **710d**.

$$M = \begin{bmatrix} M_{11} & M_{12} & M_{13} & M_{14} \\ M_{21} & M_{22} & M_{23} & M_{24} \\ M_{31} & M_{32} & M_{33} & M_{34} \\ M_{41} & M_{42} & M_{43} & M_{44} \end{bmatrix} \quad (30)$$

$$= \begin{bmatrix} HH + HV + VH + VV & HH + HV - VH - VV & 2PH + 2PV - M_{11} & 2RH + 2RV - M_{11} \\ HH - HV + VH - VV & HH - HV - VH + VV & 2PH - 2PV - M_{21} & 2RH - 2RV - M_{21} \\ 2HP + 2VP - M_{11} & 2HP - 2VP - M_{12} & 4PP - 2PH - 2PV - M_{31} & 4RP - 2RH - 2RV - M_{31} \\ 2HR + 2VR - M_{11} & 2HR - 2VR - M_{12} & 4PR - 2PH - 2PV - M_{41} & 4RR - 2RH - 2RV - M_{41} \end{bmatrix}$$

A scanning stage **711** is disposed at the second side **710b**. A mirror **712** is disposed between the scanning stage **711** and the NPBS **710**. A variable wave plate **713** is disposed between the mirror **712** and the NPBS **710**. A compensator **714** is disposed between the variable wave plate **713** and the NPBS **710**. The compensator **714** includes two quarter-wave plates and one half-wave plate. A detector **715** is disposed at the fourth side **710d**. A lens **716** is disposed between the detector **715** and the NPBS **710**. A compensator **717** is disposed between the lens **716** and the NPBS **710**. The compensator **717** includes two quarter-wave plates and one half-wave plate. A sample stage **718** is disposed at the third side **710c**. A mirror **719** is disposed between the sample stage **718** and the NPBS **710**. A sample **720** is disposed between the mirror **719** and the NPBS **710**. A dispersion compensator **721** is disposed between the sample **720** and the NPBS **710**. A controlling module **722** is coupled to the detectors **708** and **715**.

The light beam from the light source **701** is split by the NPBS **705** into two beams, where one beam is incident upon the fixed mirror **706** while the other light beam passes through the NPBS **710** and is again split into two beams, namely a reference beam **731** and a measurement beam **732**. The reference beam **731** passes through the variable wave plate **713** designed to control the polarization state and is then reflected by the mirror **712** mounted on the scanning stage **711** used to carry out path-length scanning. Meanwhile, the measurement beam **732** passes through dispersion compensator **721** used to compensate for the dispersion effect and is then incident upon the sample **720**.

The controlling module **722** calculates a Muller matrix according to signals received by the detector **708** and the

detector **715**. In detail, the signal received by the detector **708** is used for calibration, and the signal received by the detector **715** is used to obtain the intensity of the light beam. The process for the calibration and for obtaining the intensity is referred to "Measurement of Multiple Optical Parameters of Birefringent Sample Using Polarization-Sensitive Optical Coherence Tomography," by C.-C. Liao, Y.-L. Lo, and C.-Y. Yeh, *Journal of Lightwave Technology*, vol. 27, pp. 483-493, 2009, which is incorporated by reference.

To calculate the Mueller matrix of the sample **720**, the quarter-wave plate and polarizer **704** are rotated to obtain four different polarization states of the light beam incident on the sample **720**, namely H (horizontal linear polarization), V (vertical linear polarization), P (45° linear polarization), and R (right-circular polarization). In addition, the variable wave plate **713** is adjusted to change the polarization state of the reference beam **731** sequentially to H, V, P, and R, respectively, for each of the four incident lights. Thus, a total of 16 interferometric signals are produced with which to investigate the sample **720** and detected by the detector **715**. The 16 elements in the 4×4 Mueller matrix are then computed as the following equation (30).

M_{ij} is the Mueller matrix element of the i^{th} row and j^{th} column. The left and right symbols in each double polarization state notation represent the polarization states of the measurement light beam **732** and the reference light beam **731**, respectively. For example, the notation HV refers to the interferometric signal obtained given a horizontal linear polarized measurement light beam and a vertical linear polarized reference light beam.

The controlling module **722** also calculates the optical rotation angle γ and the depolarization index Δ according to the Muller matrix obtained by the equation (30). To be specific, the measurement light beam **732** passes through the sample **720** in both the forward direction and the backward direction. As shown in FIG. 7, the measurement light beam **732** is transmitted through the NPBS **710**, forward through the sample **720**, reflected from the mirror **719**, transmitted backward through the sample **720**, and finally reflected from the NPBS **710** such that it is incident on the detector **715**. Accordingly, the optical arrangement shown in FIG. 7 can be modeled using the following Mueller matrix representation.

$$M_{CB/Dep,OCT} = M_{R,BS} M_{CB/Dep} M_{Mirror} M_{CB/Dep} M_{T,BS} \quad (31)$$

M_{Mirror} is the Mueller matrix of the mirror **719**. $M_{T,BS}$ and $M_{R,BS}$ are the Mueller matrixes of the NPBS **710** in the transmission mode and reflection mode, respectively. $M_{CB/Dep}$ is the Mueller matrixes containing CB and depolarization properties. General forms of all the Mueller matrixes describing the optical components in the equation (31) are shown as the following equations (32)-(34).

$$M_{Mirror} = \begin{bmatrix} 1 & 0 & 0 & 0 \\ 0 & 1 & 0 & 0 \\ 0 & 0 & -1 & 0 \\ 0 & 0 & 0 & -1 \end{bmatrix} \quad (32)$$

$$M_{R,BS} = \begin{bmatrix} 1 & 0 & 0 & 0 \\ 0 & 1 & 0 & 0 \\ 0 & 0 & -1 & 0 \\ 0 & 0 & 0 & -1 \end{bmatrix} \quad (33)$$

$$M_{T,BS} = \begin{bmatrix} 1 & 0 & 0 & 0 \\ 0 & 1 & 0 & 0 \\ 0 & 0 & 1 & 0 \\ 0 & 0 & 0 & 1 \end{bmatrix} \quad (34)$$

Thus, the Mueller matrix of a CB/Dep sample describing the circular birefringence with the scattering effect can be expressed as the following equations (35) and (36).

$$M_{CB/Dep} = M_{CB} M_{\Delta} \quad (35)$$

$$M_{CB} = \begin{bmatrix} 1 & 0 & 0 & 0 \\ 0 & \cos(2\gamma) & \sin(2\gamma) & 0 \\ 0 & -\sin(2\gamma) & \cos(2\gamma) & 0 \\ 0 & 0 & 0 & 1 \end{bmatrix} \quad (36)$$

γ is the optical rotation angle. It is noted that the differential Mueller matrix of scattering effect can be expressed as the following equation (37).

$$m_{\Delta} = \begin{bmatrix} 0 & 0 & 0 & 0 \\ 0 & -d_1 & \eta_v & 0 \\ 0 & \eta_v & -d_2 & 0 \\ 0 & 0 & 0 & -d_3 \end{bmatrix} \quad (37)$$

d_{1-3} are the anisotropic absorptions coefficients along the x-y, 45°, and circular axes. The η_v parameter is the mean value of the nondepolarizing property. Performing an inverse differential calculation, the macroscopic Mueller matrix describing the scattering effect, M_{Δ} , can be expressed as the following equation (38).

$$M_{\Delta} = \begin{bmatrix} 1 & 0 & 0 & 0 \\ 0 & K_{22} & K_{23} & 0 \\ 0 & K_{32} & K_{33} & 0 \\ 0 & 0 & 0 & K_{44} \end{bmatrix} \quad (38)$$

The variables in the equations (36) and (38) are obtained by equating the Muller matrix of the equation (31) to that of the equation (30). For example, a genetic algorithm may be adopted to search the variables, but the invention is not limited thereto. Then, the depolarization index Δ can be calculated as the following equation (39).

$$\Delta = \sqrt{\frac{K_{22}^2 + K_{33}^2 + K_{44}^2}{3}} \quad (39)$$

Then, the controlling module 722 calculates a glucose concentration corresponding to the sample according to the optical rotation angle and the depolarization index.

FIG. 8 is a diagram illustrating relationship between the depolarization index and the optical path length. First, an optical path length is obtained in accordance with the depolarization index. Referring to FIG. 8, The Rayleigh model describes scattering of light by particles whose size is much smaller than the wavelength of the light. For arbitrary values of the mean free path (l) and the length of the sample (L), some rays (i.e. light beams) may pass through the sample without undergoing bulk scattering. The fraction of “unscattered” rays (or the depolarization index) can be determined from the fact that rays which travel a distance x within the sample have an integrated probability of having been scattered given by the following equation (40).

$$p(x) = 1.0 - e^{-x/l} \quad (40)$$

Thus, the integrated probability of a ray travelling a distance x within the sample and not undergoing scattering is given by the following equation (41).

$$1 - p(x) = e^{-x/l} \quad (41)$$

Setting $x=L$, we find that the probability of a ray traveling through the full sample and not being scattered is as the following equation (42). That is, the optical path length (l) is obtained by substituting the depolarization index into the equation (42).

$$\Delta = e^{-L/l} \quad (42)$$

The extracted values of glucose concentration are obtained by the following equation (43).

$$C = \frac{\gamma}{[\gamma]_T^\lambda l} \quad (43)$$

where γ is the experimental value of the optical rotation angle. l is the optical path length obtained from the equation (40). $[\gamma]_T^\lambda$ is the optical rotation angle of the sample at room temperature T and wavelength λ of the light beam obtained from “New optical scheme for a polarimetric based glucose sensor” by R. R. Ansari, S. Bockle and L. Rovati, J. Biomed. Opt. 9, pp. 103-115 (2204). Referring to FIG. 9, the predicted glucose concentration is close to the actual glucose concentration. Note that the equations (40)-(43) may be applied to the embodiments of FIG. 1 to FIG. 6.

Although the present invention has been described in considerable detail with reference to certain embodiments thereof, other embodiments are possible. Therefore, the spirit and scope of the appended claims should not be limited to the description of the embodiments contained herein. It will be apparent to those skilled in the art that various modifications and variations can be made to the structure of the present invention without departing from the scope or spirit of the invention. In view of the foregoing, it is intended that the present invention cover modifications and variations of this invention provided they fall within the scope of the following claims.

What is claimed is:

1. A system for sensing glucose concentration, the system comprising:
 - a light source configured to generate a light beam;
 - a polarization state generator configured to receive the light beam, wherein the polarization state generator comprises a modulator for changing a polarization of

the light beam, and the light beam passing the modulator is emitted to a biological tissue;
 a polarization state analyzer configured to receive the light beam reflected from the biological tissue; and
 a controlling module configured to transmit an electrical signal to the modulator, wherein the electrical signal has n sampling points which correspond to n polarizations of the light beam respectively, the n polarizations are different from each other, and n is a positive integer greater than or equal to 4,
 wherein for each of the n sampling points, the controlling module calculates a Stokes vector according to the light beam received by the polarization state analyzer,
 wherein the controlling module calculates a Mueller matrix according to the Stokes vectors corresponding to the n sampling points, and calculates at least one parameter according to the Mueller matrix, wherein the at least one parameter comprises a depolarization index or an optical rotation angle,
 wherein the controlling module calculates a glucose concentration corresponding to the biological tissue according to the at least one parameter.

2. The system of claim 1, wherein the polarization state generator further comprises:

a polarizer disposed between the modulator and the light source, wherein a principal axis of the polarizer is 0°; and
 a quarter-wave plate disposed between the modulator and the biological tissue, wherein a principal axis of the quarter-wave plate is 0°,
 wherein a principal axis of the modulator is 45°.

3. The system of claim 1, wherein the polarization state generator further comprises:

a polarizer disposed between the modulator and the light source;
 a quarter-wave plate disposed between the modulator and the biological tissue; and
 a half-wave plate disposed between the quarter-wave plate and the biological tissue.

4. The system of claim 3, wherein the modulator is an electro-optic modulator, a principal axis of the polarizer is 0°, a principal axis of the electro-optic modulator is 45°, a principal axis of the quarter-wave plate is 45°, and a principal axis of the half-wave plate is 45°,

wherein a Stokes vector of the light beam emitted by the polarization state generator is represented by following equations (1) and (2):

$$S' = \begin{bmatrix} 1 \\ \cos a \\ \sin a \\ 1 \end{bmatrix} \quad (1)$$

$$a = \frac{\pi V}{V_{\lambda/2}} \quad (2)$$

wherein S' is the Stokes vector of the light beam emitted by the polarization state generator, V is a constant, $V_{\lambda/2}$ is an amplitude of the electrical signal.

5. The system of claim 4, wherein the polarization state analyzer comprises:

a second electro-optic modulator with a principal axis of 0°;

a third electro-optic modulator with a principal axis of 45°, wherein the second electro-optic modulator is disposed between the biological tissue and the third electro-optic modulator;

an analyzer with a principal axis of 0°; and

a detector, wherein the analyzer is disposed between the third electro-optic modulator and the detector, and the detector is configured to receive the light beam passing through the second electro-optic modulator, the third electro-optic modulator, and the analyzer.

6. The system of claim 5, wherein the controlling module performs a Fourier transform on brightness of the light beam received by the detector to obtain a plurality of brightness parameters, and calculates a plurality of Stokes parameters of the corresponding Stokes vector according to the plurality of brightness parameters.

7. The system of claim 6, wherein the controlling module calculates a differential Mueller matrix according to following equations (3) and (4):

$$\lambda_m = \ln(\lambda_M)/z \quad (3)$$

$$m = V_M m_\lambda V_M^{-1} = \begin{bmatrix} m_{11} & m_{12} & m_{13} & m_{14} \\ m_{21} & m_{22} & m_{23} & m_{24} \\ m_{31} & m_{32} & m_{33} & m_{34} \\ m_{41} & m_{42} & m_{43} & m_{44} \end{bmatrix} \quad (4)$$

wherein z represents a direction that the light beam propagates along, m is the differential Mueller matrix, V_M represents eigenvectors of the Mueller matrix, λ_M represents eigenvalues of the Mueller matrix, λ_m represents eigenvalues of the differential Mueller matrix, m_λ is a diagonal matrix constituted by the eigenvalues λ_m , and the optical rotation angle is represented as $\gamma = (m_{23} - m_{32})/4$.

8. The system of claim 7, wherein the controlling module generates a differential Mueller matrix m_Δ as a following equation (5) according to the differential Mueller matrix m:

$$m_\Delta = \begin{bmatrix} 0 & \frac{(m_{12} - m_{21})}{2} & \frac{(m_{13} - m_{31})}{2} & \frac{(m_{14} - m_{41})}{2} \\ \frac{(m_{21} - m_{12})}{2} & m_{22} - m_{11} & \frac{(m_{23} + m_{32})}{2} & \frac{(m_{24} + m_{42})}{2} \\ \frac{(m_{31} - m_{13})}{2} & \frac{(m_{23} + m_{32})}{2} & m_{33} - m_{11} & \frac{(m_{34} + m_{43})}{2} \\ \frac{(m_{41} - m_{14})}{2} & \frac{(m_{24} + m_{42})}{2} & \frac{(m_{34} + m_{43})}{2} & m_{44} - m_{11} \end{bmatrix} \quad (5)$$

the controlling module substitutes the differential Mueller matrix m_Δ into the equation (4) to calculate a Mueller matrix M_Δ as a following equation (6):

$$M_\Delta = \begin{bmatrix} 1 & K_{12} & K_{13} & K_{14} \\ -K_{12} & K_{22} & K_{23} & K_{24} \\ -K_{13} & K_{23} & K_{33} & K_{34} \\ -K_{14} & K_{24} & K_{34} & K_{44} \end{bmatrix} \quad (6)$$

wherein the depolarization index is represented as a following equation (7):

$$\Delta = 1 - \sqrt{\frac{K_{22}^2 + K_{33}^2 + K_{44}^2}{3}} \quad (7)$$

9. The system of claim 8, wherein the controlling module substitutes the optical rotation angle into a linearly increasing function to obtain the glucose concentration, or substitutes the depolarization index into a linearly decreasing function to obtain the glucose concentration.

10. The system of claim 8, wherein the controlling module obtains an optical path length in accordance with a following equation (8):

$$\Delta = e^{-L/l} \quad (8)$$

wherein Δ is the depolarization index, L is a length of the sample, and l is the optical path length,

wherein the controlling module calculates the glucose concentration corresponding to the sample in accordance with a following equation (9):

$$C = \frac{\gamma}{[\gamma]_T^\lambda} l \quad (9)$$

where C is the glucose concentration, γ is the optical rotation angle, $[\gamma]_T^\lambda$ is the optical rotation angle of the sample at room temperature T , and λ is a wavelength of the light beam.

11. A method for sensing glucose concentration for a system which comprises a light source, a polarization state generator and a polarization state analyzer, wherein a light beam generated by the light source is emitted to the polarization state generator and then is emitted to a biological tissue, the polarization state analyzer receives the light beam reflected from the biological tissue, and the method comprises:

transmitting an electrical signal to a modulator of the polarization state generator, wherein the electrical signal has n sampling points which correspond to n polarizations of the light beam respectively, the n polarizations are different from each other, and n is a positive integer greater than or equal to 4;

calculating a Stokes vector according to the light beam received by the polarization state analyzer for each of the n sampling points; and

calculating a Mueller matrix according to the Stokes vectors corresponding to the n sampling points, calculating at least one parameter according to the Mueller matrix, and calculating a glucose concentration corresponding to the biological tissue according to the at least one parameter, wherein the at least one parameter comprises a depolarization index or an optical rotation angle.

12. A system for sensing glucose concentration, the system comprising:

a light source configured to generate a light beam; an optical coherence tomography (OCT) device configured to receive the light beam, wherein the optical coherence tomography comprises at least one detector; and

a controlling module, calculating a Muller matrix according to signals received by the at least one detector, and calculating an optical rotation angle and a depolarization index according to the Muller matrix, and calcu-

lating a glucose concentration corresponding to a sample according to the optical rotation angle and the depolarization index.

13. The system of claim 12, wherein the optical coherence tomography device comprises:

a polarization state generator, configured to receive the light beam and change a polarization of the light beam; a first detecting module, configured to compensate the light beam and split the light beam;

a second detecting module, coupled to the first detecting module and configured to split the light beam;

a reference arm, disposed at a side of the second detecting module; and

a measurement arm, disposed at another side of the second detecting module.

14. The system of claim 13,

wherein the polarization stage generator comprises:

a polarizer and a quarter-wave plate, configured to receive light; and

a plurality of first lens disposed between the light source and the polarizer and the quarter-wave plate, wherein the first detecting module comprises:

a first non-polarizing beam splitter (NPBS) having a first side, a second side, a third side and a fourth side, wherein the first side is opposite to the third side, the second side is opposite to the fourth side, and the polarizer and the quarter-wave plate are disposed at the first side of the first NPBS;

a first mirror, disposed at the second side of the first NPBS;

a first dispersion compensator disposed between the first mirror and the first NPBS;

a first detector, disposed at the fourth side of the first NPBS;

a second lens disposed between the first NPBS and the first detector,

wherein the second detecting module comprises:

a second NPBS, disposed at the third side of the first NPBS and having a first side, a second side, a third side and a fourth side, wherein the first side of the second NPBS is opposite to the third side of the second NPBS, the second side of the second NPBS is opposite to the fourth side of the second NPBS;

a second detector, disposed at the fourth side of the second NPBS;

a third lens, disposed between the second NPBS and the second detector; and

a first compensator, disposed between the second NPBS and the third lens,

wherein the reference arm comprises:

a scanning stage, disposed at the second side of the second NPBS;

a second mirror, disposed between the scanning stage and the second NPBS;

a variable wave plater, disposed between the second mirror and the second NPBS; and

a second compensator, disposed between the second NPBS and the variable wave plater,

wherein the measurement arm comprises:

a sample stage, disposed at the third side of the second NPBS;

a third mirror, disposed between the second NPBS and the sample stage;

the sample, disposed between the third mirror and the second NPBS; and

a second dispersion compensator, disposed between the second NPBS and the sample.

15. The system of claim 14, wherein the first compensator comprises two quarter-wave plates and one half-wave plate, wherein the second compensator comprises two quarter-wave plates and one half-wave plate.

16. The system of claim 15, wherein the controlling module rotates the quarter-wave plate and the polarizer, and adjusts the variable wave plate to produce at least 16 interferometric signals detected by the second detector, wherein the controlling module calculates the Muller matrix according to the 16 interferometric signals.

17. The system of claim 16, wherein the controlling module obtains an optical path length in accordance with a following equation (1):

$$\Delta = e^{-L/l} \quad (1)$$

wherein Δ is the depolarization index, L is a length of the sample, and l is the optical path length, wherein the controlling module calculates the glucose concentration corresponding to the sample in accordance with a following equation (2):

$$C = \frac{\gamma}{[\gamma]_T^{\lambda} l} \quad (2)$$

where C is the glucose concentration, γ is the optical rotation angle, $[\gamma]_T^{\lambda}$ is the optical rotation angle of the sample at room temperature T , and λ is a wavelength of the light beam.

* * * * *

专利名称(译)	用于感测葡萄糖浓度的方法和系统		
公开(公告)号	US10188332	公开(公告)日	2019-01-29
申请号	US15/862611	申请日	2018-01-04
[标]申请(专利权)人(译)	国立成功大学		
申请(专利权)人(译)	成大		
当前申请(专利权)人(译)	成大		
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发明人	LO, YU-LUNG PHAN, QUOC-HUNG LIAO, CHIA-CHI		
IPC分类号	G01J4/00 A61B5/1455 A61B5/145 A61B5/00 G01J3/447 A61B3/10		
CPC分类号	A61B5/14558 A61B3/102 G01J3/447 A61B5/14532 A61B5/7235 A61B5/0066 A61B2562/0233 G01J4/04		
优先权	106105137 2017-02-16 TW		
其他公开文献	US20180228415A1		
外部链接	Espacenet		

摘要(译)

提供了一种用于感测葡萄糖浓度的系统，其包括以下组件。光源产生光束。该系统可以包括用于改变光束的偏振的偏振态发生器 (PSG)，然后将光束发射到生物组织。偏振态分析器 (PSA) 接收从生物组织反射的光束，并且接收的光束用于计算斯托克斯矢量。根据斯托克斯矢量计算穆勒矩阵。在一些实施例中，该系统包括光学相干断层摄影术 (OCT)，其中光束由检测器感测以计算穆勒矩阵。根据差分穆勒矩阵形式计算光学旋转角度和消偏振指数。根据旋光角度和消偏指数计算葡萄糖浓度。

