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(54) **ULTRASOUND PROBE FOR TREATING SKIN LAXITY**

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(56) **References Cited**

U.S. PATENT DOCUMENTS

2,427,348 A 9/1947 Bond et al.
2,792,829 A 2/1952 Calosi

(Continued)

FOREIGN PATENT DOCUMENTS

CN 104027893 9/2014
DE 4029175 3/1992

(Continued)

OTHER PUBLICATIONS

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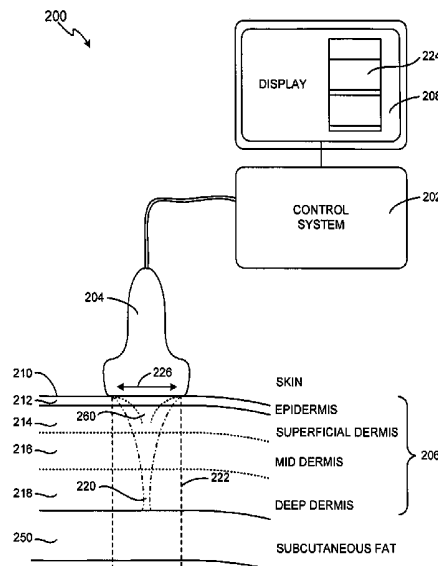
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(57) **ABSTRACT**

A probe for ultrasound treatment of skin laxity are provided. Systems and methods can include ultrasound imaging of the region of interest for localization of the treatment area, delivering ultrasound energy at a depth and pattern to achieve the desired therapeutic effects, and/or monitoring the treatment area to assess the results and/or provide feedback. In an embodiment, a treatment system and method can be configured for producing arrays of sub-millimeter and larger zones of thermal ablation to treat the epidermal, superficial dermal, mid-dermal or deep dermal components of tissue.

20 Claims, 22 Drawing Sheets



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See application file for complete search history.

(56) References Cited**U.S. PATENT DOCUMENTS**

3,913,386 A 10/1975 Saglio
 3,965,455 A 6/1976 Hurwitz
 3,992,925 A 11/1976 Perilhou
 4,039,312 A 8/1977 Patru
 4,059,098 A 11/1977 Murdock
 4,101,795 A 7/1978 Fukumoto
 4,151,834 A 5/1979 Sato et al.
 4,166,967 A 9/1979 Benes et al.
 4,211,948 A 7/1980 Smith et al.
 4,211,949 A 7/1980 Briskin et al.
 4,213,344 A 7/1980 Rose
 4,276,491 A 6/1981 Daniel
 4,315,514 A 2/1982 Drewes et al.
 4,325,381 A 4/1982 Glenn
 4,343,301 A 8/1982 Indech

4,372,296 A 2/1983 Fahim
 4,379,145 A 4/1983 Masuho et al.
 4,381,007 A 4/1983 Doss
 4,381,787 A 5/1983 Hottinger
 4,397,314 A 8/1983 Vaguine
 4,409,839 A 10/1983 Taenzer
 4,431,008 A 2/1984 Wanner et al.
 4,441,486 A 4/1984 Pounds
 4,452,084 A 6/1984 Taenzer
 4,484,569 A 11/1984 Driller
 4,507,582 A 3/1985 Glenn
 4,513,749 A 4/1985 Kino
 4,513,750 A 4/1985 Heyman et al.
 4,527,550 A 7/1985 Ruggera et al.
 4,528,979 A 7/1985 Marchenko
 4,534,221 A 8/1985 Fife et al.
 4,566,459 A 1/1986 Umemura et al.
 4,567,895 A 2/1986 Putzke
 4,586,512 A 5/1986 Do-Huu
 4,601,296 A 7/1986 Yerushalmi
 4,620,546 A 11/1986 Aida et al.
 4,637,256 A 1/1987 Sugiyama et al.
 4,646,756 A 3/1987 Watmough
 4,663,358 A 5/1987 Hyon
 4,668,516 A 5/1987 Duraffourd et al.
 4,672,591 A 6/1987 Breimesser et al.
 4,680,499 A 7/1987 Umemura et al.
 4,697,588 A 10/1987 Reichenberger
 4,754,760 A 7/1988 Fukukita et al.
 4,757,820 A 7/1988 Itoh
 4,771,205 A 9/1988 Mequio
 4,801,459 A 1/1989 Liburdy
 4,803,625 A 2/1989 Fu et al.
 4,807,633 A 2/1989 Fry
 4,817,615 A 4/1989 Fukukita et al.
 4,858,613 A 8/1989 Fry
 4,860,732 A 8/1989 Hasegawa et al.
 4,865,041 A 9/1989 Hassler
 4,865,042 A 9/1989 Umemura
 4,867,169 A 9/1989 Machida
 4,874,562 A 10/1989 Hyon
 4,875,487 A 10/1989 Seppi
 4,881,212 A 11/1989 Takeuchi
 4,891,043 A 1/1990 Zeimer et al.
 4,893,624 A 1/1990 Lele
 4,896,673 A 1/1990 Rose
 4,900,540 A 2/1990 Ryan et al.
 4,901,729 A 2/1990 Saitoh
 4,917,096 A 4/1990 Englehart
 4,932,414 A 6/1990 Coleman et al.
 4,938,216 A 7/1990 Lele
 4,938,217 A 7/1990 Lele
 4,947,046 A 8/1990 Kawabata et al.
 4,951,653 A 8/1990 Fry
 4,955,365 A 9/1990 Fry
 4,958,626 A 9/1990 Nambu
 4,976,709 A 12/1990 Sand
 4,979,501 A 12/1990 Valchanov
 4,992,989 A 2/1991 Watanabe et al.
 5,012,797 A 5/1991 Liang
 5,018,508 A 5/1991 Fry et al.
 5,030,874 A 7/1991 Saito et al.
 5,036,855 A 8/1991 Fry
 5,040,537 A 8/1991 Katakura
 5,054,310 A 10/1991 Flynn
 5,054,470 A 10/1991 Fry
 5,054,491 A 10/1991 Saito et al.
 5,070,879 A 12/1991 Herres
 5,088,495 A 2/1992 Miyagawa
 5,115,814 A 5/1992 Griffith
 5,117,832 A 6/1992 Sanghvi
 5,123,418 A 6/1992 Saurel
 5,142,511 A 8/1992 Kanai et al.
 5,143,063 A 9/1992 Fellner
 5,143,074 A 9/1992 Dory
 5,149,319 A 9/1992 Unger
 5,150,711 A 9/1992 Dory
 5,150,714 A 9/1992 Green
 5,152,294 A 10/1992 Mochizuki et al.

(56)

References Cited

U.S. PATENT DOCUMENTS

5,156,144 A	10/1992	Iwasaki	5,523,058 A	6/1996	Umemura et al.
5,158,536 A	10/1992	Sekins	5,524,620 A	6/1996	Rosenchein
5,159,931 A	11/1992	Pini	5,524,624 A	6/1996	Tepper
5,163,421 A	11/1992	Bernstein	5,524,625 A	6/1996	Okazaki
5,163,436 A	11/1992	Saitoh et al.	5,526,624 A	6/1996	Berg
5,178,135 A	1/1993	Uchiyama et al.	5,526,812 A	6/1996	Dumoulin et al.
5,190,518 A	3/1993	Takasu	5,526,814 A	6/1996	Cline et al.
5,190,766 A	3/1993	Ishihara	5,526,815 A	6/1996	Granz
5,191,880 A	3/1993	McLeod	5,529,070 A	6/1996	Augustine et al.
5,205,287 A	4/1993	Erbel et al.	5,540,235 A	7/1996	Wilson
5,209,720 A	5/1993	Unger	5,558,092 A	9/1996	Unger
5,212,671 A	5/1993	Fujii et al.	5,560,362 A	10/1996	Sliwa et al.
5,215,680 A	6/1993	D'Arrigo	5,573,497 A	11/1996	Chapelon
5,224,467 A	7/1993	Oku	5,575,291 A	11/1996	Hayakawa
5,230,334 A	7/1993	Klopotek	5,575,807 A	11/1996	Faller
5,230,338 A	7/1993	Allen et al.	5,577,502 A	11/1996	Darrow et al.
5,247,924 A	9/1993	Suzuki et al.	5,577,507 A	11/1996	Snyder et al.
5,255,681 A	10/1993	Ishimura et al.	5,577,991 A	11/1996	Akui et al.
5,257,970 A	11/1993	Dougherty	5,580,575 A	12/1996	Unger et al.
5,265,614 A	11/1993	Hayakawa	5,601,526 A *	2/1997	Chapelon A61N 7/02 601/2
5,267,985 A	12/1993	Shimada	5,603,323 A	2/1997	Pflugrath et al.
5,269,297 A	12/1993	Weng	5,605,154 A *	2/1997	Ries G01S 7/52046 600/444
5,282,797 A	2/1994	Chess	5,609,562 A	3/1997	Kaali
5,295,484 A	3/1994	Marcus	5,615,091 A	3/1997	Palatnik
5,295,486 A	3/1994	Wollschlager et al.	5,618,275 A	4/1997	Bock
5,304,169 A	4/1994	Sand	5,620,479 A	4/1997	Diederich
5,305,756 A	4/1994	Entrekin et al.	5,622,175 A	4/1997	Sudol et al.
5,321,520 A	6/1994	Inga et al.	5,617,858 A	5/1997	Taverna et al.
5,323,779 A	6/1994	Hardy et al.	5,638,819 A	6/1997	Manwaring et al.
5,327,895 A	7/1994	Hashimoto et al.	5,643,179 A *	7/1997	Fujimoto A61N 7/02 601/2
5,329,202 A	7/1994	Garlick et al.	5,644,085 A	7/1997	Lorraine et al.
5,348,016 A	9/1994	Unger et al.	5,647,373 A	7/1997	Paltiel
5,358,466 A *	10/1994	Aida A61B 17/2256 600/439	5,655,535 A	8/1997	Frlemel et al.
5,360,268 A	11/1994	Hayashi	5,655,538 A	8/1997	Lorraine
5,370,121 A	12/1994	Reichenberger	5,657,760 A	8/1997	Ying
5,370,122 A	12/1994	Kunig	5,658,328 A	8/1997	Johnson
5,371,483 A	12/1994	Bhardwaj	5,660,836 A *	8/1997	Knowlton A61B 18/12 128/898
5,375,602 A	12/1994	Lancee et al.	5,662,116 A	9/1997	Kondo
5,379,773 A	1/1995	Hornsby	5,665,053 A	9/1997	Jacobs
5,380,280 A	1/1995	Peterson	5,665,141 A	9/1997	Vago
5,380,519 A	1/1995	Schneider et al.	5,671,746 A	9/1997	Dreschel et al.
5,383,917 A	1/1995	Desai et al.	5,673,699 A	10/1997	Trahey et al.
5,391,140 A	2/1995	Schaetzle et al.	5,676,692 A	10/1997	Sanghvi
5,391,197 A	2/1995	Burdette et al.	5,685,820 A	11/1997	Riek et al.
5,392,259 A	2/1995	Bolorforosh	5,690,608 A	11/1997	Watanabe
5,396,143 A	3/1995	Seyed-Bolorforosh et al.	5,694,936 A	12/1997	Fujimoto
5,398,689 A	3/1995	Connor et al.	5,697,897 A	12/1997	Buchholtz
5,406,503 A	4/1995	Williams	5,701,900 A	12/1997	Shehada et al.
5,413,550 A *	5/1995	Castel A61H 23/0245 601/2	5,704,361 A	1/1998	Seward et al.
5,417,216 A	5/1995	Tanaka	5,706,252 A	1/1998	Le Verrier et al.
5,423,220 A	6/1995	Finsterwald et al.	5,706,564 A	1/1998	Rhyne
5,435,311 A	7/1995	Umemura	5,715,823 A	2/1998	Wood et al.
5,438,998 A	8/1995	Hanafy	5,720,287 A	2/1998	Chapelon et al.
5,443,068 A *	8/1995	Cline A61B 5/0555 600/411	5,722,411 A	3/1998	Suzuki
5,445,611 A	8/1995	Eppstein et al.	5,727,554 A	3/1998	Kalend et al.
5,458,596 A	10/1995	Lax	5,735,280 A	4/1998	Sherman et al.
5,460,179 A	10/1995	Okunuki et al.	5,743,863 A	4/1998	Chapelon
5,460,595 A	10/1995	Hall et al.	5,746,005 A	5/1998	Steinberg
5,419,327 A	11/1995	Rohwedder	5,746,762 A	5/1998	Bass
5,469,854 A	11/1995	Unger et al.	5,748,767 A	5/1998	Raab
5,471,488 A	12/1995	Fujio	5,749,364 A	5/1998	Sliwa et al.
5,472,405 A	12/1995	Buchholtz et al.	5,755,228 A	5/1998	Wilson et al.
5,487,388 A	1/1996	Rello et al.	5,755,753 A	5/1998	Knowlton
5,492,126 A	2/1996	Hennige	5,762,066 A	6/1998	Law
5,496,256 A	3/1996	Bock	5,763,886 A	6/1998	Schulte
5,501,655 A	3/1996	Rolt	5,769,790 A	6/1998	Watkins
5,503,152 A	4/1996	Oakley et al.	5,779,644 A	7/1998	Eberle et al.
5,503,320 A	4/1996	Webster et al.	5,792,058 A	8/1998	Lee
5,507,790 A	4/1996	Weiss	5,795,297 A	8/1998	Daigle
5,511,296 A	4/1996	Dias et al.	5,795,311 A	8/1998	Wess
5,520,188 A	5/1996	Hennige	5,810,009 A	9/1998	Mine et al.
5,522,869 A	6/1996	Burdette	5,810,888 A	9/1998	Fenn
			5,814,599 A	9/1998	Mitragotri et al.
			5,817,013 A	10/1998	Ginn et al.
			5,817,021 A	10/1998	Reichenberger

(56)

References Cited

U.S. PATENT DOCUMENTS

5,820,564 A	10/1998	Slayton	6,159,150 A	12/2000	Yale et al.
5,823,962 A	10/1998	Schaetzle	6,171,244 B1	1/2001	Finger et al.
5,827,204 A	10/1998	Grandia et al.	6,176,840 B1	1/2001	Nishimura
5,840,032 A	11/1998	Hatfield et al.	6,183,426 B1	2/2001	Akisada
5,844,140 A	12/1998	Seale	6,183,502 B1	2/2001	Takeuchi
5,853,367 A	12/1998	Chalek et al.	6,183,773 B1	2/2001	Anderson
5,869,751 A	2/1999	Bonin	6,190,323 B1	2/2001	Dias
5,871,524 A	2/1999	Knowlton	6,190,336 B1	2/2001	Duarte
5,873,902 A	2/1999	Sanghvi	6,193,658 B1	2/2001	Wendelken
5,876,341 A	3/1999	Wang et al.	6,198,956 B1	3/2001	Dunne
5,879,303 A	3/1999	Averkiou et al.	6,210,327 B1	4/2001	Brackett et al.
5,882,557 A	3/1999	Hayakawa	6,213,948 B1	4/2001	Barthe
5,891,034 A	4/1999	Bucholz	6,216,029 B1	4/2001	Paltieli
5,895,356 A	4/1999	Andrus et al.	6,233,476 B1	5/2001	Strommer et al.
5,899,861 A	5/1999	Friemel et al.	6,234,990 B1	5/2001	Rowe et al.
5,904,659 A	5/1999	Duarte	6,241,753 B1 *	6/2001	Knowlton A61B 18/12 128/898
5,919,219 A	7/1999	Knowlton	6,246,898 B1	6/2001	Vesely et al.
5,923,099 A	7/1999	Bilir	6,251,074 B1	6/2001	Averkiou et al.
5,924,989 A	7/1999	Polz	6,251,088 B1	6/2001	Kaufman et al.
5,928,169 A	7/1999	Schatzle et al.	6,268,405 B1	7/2001	Yao
5,931,805 A	8/1999	Brisken	6,273,864 B1	8/2001	Duarte
5,938,606 A	8/1999	Bonnefous	6,280,402 B1	8/2001	Ishibashi et al.
5,938,612 A	8/1999	Kline-Schoder	6,287,257 B1	9/2001	Maticchuk
5,948,011 A	9/1999	Knowlton	6,287,304 B1	9/2001	Eggers et al.
5,957,844 A	9/1999	Dekel	6,296,619 B1	10/2001	Brisken
5,957,882 A	9/1999	Nita et al.	6,301,989 B1	10/2001	Brown et al.
5,957,941 A	9/1999	Ream	6,307,302 B1	10/2001	Toda
5,964,707 A	10/1999	Fenster et al.	6,309,355 B1	10/2001	Cain et al.
5,967,980 A	10/1999	Ferre et al.	6,311,090 B1	10/2001	Knowlton
5,968,034 A	10/1999	Fullmer	6,315,741 B1 *	11/2001	Martin A61B 8/4254 601/3
5,971,949 A	10/1999	Levin	6,322,509 B1	11/2001	Pan et al.
5,977,538 A	11/1999	Unger et al.	6,322,532 B1	11/2001	D'Sa
5,984,881 A *	11/1999	Ishibashi A61B 17/2256 601/2	6,325,540 B1	12/2001	Lounsberry et al.
5,984,882 A	11/1999	Rosenchein	6,325,758 B1	12/2001	Carol et al.
5,990,598 A	11/1999	Sudol et al.	6,325,769 B1	12/2001	Klopotek
5,997,471 A	12/1999	Gumb et al.	6,325,798 B1	12/2001	Edwards et al.
5,997,497 A	12/1999	Nita et al.	6,350,276 B1	2/2002	Knowlton
5,999,843 A	12/1999	Anbar	6,356,780 B1	3/2002	Licato et al.
6,004,262 A	12/1999	Putz et al.	6,361,531 B1	3/2002	Hissong
6,007,499 A	12/1999	Martin et al.	6,370,411 B1	4/2002	Osadchy et al.
6,013,032 A	1/2000	Savord	6,375,672 B1	4/2002	Aksan
6,014,473 A	1/2000	Hossack et al.	6,377,854 B1	4/2002	Knowlton
6,016,255 A	1/2000	Bolan et al.	6,377,855 B1	4/2002	Knowlton
6,019,724 A	2/2000	Gronningsaeter et al.	6,381,497 B1	4/2002	Knowlton
6,022,308 A	2/2000	Williams	6,381,498 B1	4/2002	Knowlton
6,022,317 A	2/2000	Cruanas et al.	6,387,380 B1	5/2002	Knowlton
6,022,327 A	2/2000	Chang	6,390,982 B1	5/2002	Bova et al.
6,030,374 A	2/2000	McDaniel	6,405,090 B1	6/2002	Knowlton
6,036,646 A	3/2000	Barthe	6,409,720 B1	6/2002	Hissong
6,039,048 A	3/2000	Silberg	6,413,216 B1	7/2002	Cain et al.
6,039,689 A	3/2000	Lizzi	6,413,253 B1	7/2002	Koop
6,042,556 A *	3/2000	Beach A61N 7/02 600/437	6,413,254 B1	7/2002	Hissong
6,049,159 A	4/2000	Barthe	6,419,648 B1	7/2002	Vitek
6,050,943 A	4/2000	Slayton	6,423,007 B2	7/2002	Lizzi et al.
6,059,727 A	5/2000	Fowlkes	6,425,865 B1	7/2002	Salcudean
6,071,239 A	6/2000	Cribbs	6,425,867 B1	7/2002	Vaezy
6,080,108 A	6/2000	Dunham	6,425,912 B1	7/2002	Knowlton
6,083,148 A	7/2000	Williams	6,428,477 B1	8/2002	Mason
6,086,535 A	7/2000	Ishibashi	6,428,532 B1	8/2002	Doukas
6,086,580 A	7/2000	Mordon et al.	6,430,446 B1	8/2002	Knowlton
6,090,054 A	7/2000	Tagishi	6,432,057 B1	8/2002	Mazess et al.
6,093,148 A *	7/2000	Fujimoto A61N 7/00 600/438	6,432,067 B1	8/2002	Martin
6,093,883 A	7/2000	Sanghvi	6,432,101 B1	8/2002	Weber
6,101,407 A	8/2000	Groezinger	6,436,061 B1	8/2002	Costantino
6,106,469 A	8/2000	Suzuki et al.	6,438,424 B1	8/2002	Knowlton
6,113,558 A	9/2000	Rosenchein	6,440,071 B1	8/2002	Slayton
6,113,559 A	9/2000	Klopotek	6,440,121 B1	8/2002	Weber
6,120,452 A	9/2000	Barthe	6,443,914 B1	9/2002	Costantino
6,123,081 A	9/2000	Durette	6,447,443 B1	9/2002	Keogh et al.
6,126,619 A	10/2000	Peterson et al.	6,451,013 B1	9/2002	Bays et al.
6,135,971 A	10/2000	Hutchinson	6,453,202 B1	9/2002	Knowlton
6,139,499 A	10/2000	Wilk	6,461,304 B1	10/2002	Tanaka et al.
			6,461,378 B1	10/2002	Knowlton
			6,470,216 B1	10/2002	Knowlton
			6,338,716 B1	11/2002	Hossack et al.
			6,488,626 B1	12/2002	Lizzi
			6,491,657 B2	12/2002	Rowe

(56)

References Cited

U.S. PATENT DOCUMENTS

6,500,121	B1	12/2002	Slayton	6,997,923	B2	2/2006	Anderson
6,500,141	B1	12/2002	Irion	7,006,874	B2	2/2006	Knowlton
6,506,171	B1	1/2003	Vitek et al.	7,020,528	B2	3/2006	Neev
6,508,774	B1	1/2003	Acker	7,022,089	B2	4/2006	Ooba
6,511,427	B1	1/2003	Sliwa, Jr. et al.	7,058,440	B2	6/2006	Heuscher et al.
6,511,428	B1	1/2003	Azuma	7,063,666	B2	6/2006	Weng
6,514,244	B2	2/2003	Pope	7,070,565	B2	7/2006	Vaezy et al.
6,517,484	B1	2/2003	Wilk	7,074,218	B2	7/2006	Washington et al.
6,524,250	B1	2/2003	Weber	7,094,252	B2	8/2006	Koop
6,666,835	B2	3/2003	Martin	7,108,663	B2	9/2006	Talish et al.
6,540,679	B2	4/2003	Slayton	7,115,123	B2	10/2006	Knowlton
6,540,685	B1	4/2003	Rhoads et al.	7,122,029	B2	10/2006	Koop et al.
6,540,700	B1	4/2003	Fujimoto et al.	7,142,905	B2	11/2006	Slayton
6,547,788	B1	4/2003	Maguire et al.	7,165,451	B1	1/2007	Brooks et al.
6,554,771	B1	4/2003	Buil et al.	7,179,238	B2	2/2007	Hissong
6,569,099	B1	5/2003	Babaev	7,189,230	B2	3/2007	Knowlton
6,569,108	B2	5/2003	Sarvazyan et al.	7,229,411	B2	6/2007	Slayton
6,572,552	B2	6/2003	Fukukita	7,235,592	B2	6/2007	Muratoglu
6,575,956	B1	6/2003	Brisken et al.	7,258,674	B2	8/2007	Cribbs
6,595,934	B1	7/2003	Hissong	7,273,459	B2	9/2007	Desilets
6,599,256	B1	7/2003	Acker	7,294,125	B2	11/2007	Phalen et al.
6,605,043	B1	8/2003	Dreschel	7,297,117	B2	11/2007	Trucco
6,605,080	B1	8/2003	Altshuler et al.	7,303,555	B2	12/2007	Makin et al.
6,607,498	B2	8/2003	Eshel	7,311,679	B2	12/2007	Desilets et al.
6,618,620	B1	9/2003	Freundlich et al.	7,327,071	B2	2/2008	Nishiyama et al.
6,623,430	B1	9/2003	Slayton	7,331,951	B2	2/2008	Eshel et al.
6,626,854	B2	9/2003	Friedman	7,332,985	B2	2/2008	Larson et al.
6,626,855	B1	9/2003	Weng	7,338,434	B1	3/2008	Haarstad et al.
6,638,226	B2	10/2003	He et al.	7,347,855	B2	3/2008	Eshel
6,645,150	B2	11/2003	Angelsen et al.	RE40,403	E	6/2008	Cho et al.
6,645,162	B2	11/2003	Friedman	7,393,325	B2	7/2008	Barthe
6,662,054	B2	12/2003	Kreindel	7,398,116	B2	7/2008	Edwards
6,663,627	B2	12/2003	Francischelli	7,399,279	B2	7/2008	Abend et al.
6,665,806	B1	12/2003	Shimizu	7,491,171	B2	2/2009	Barthe et al.
6,669,638	B1	12/2003	Miller	7,507,235	B2	3/2009	Keogh et al.
6,685,639	B1	2/2004	Wang et al.	7,510,536	B2	3/2009	Foley et al.
6,685,640	B1	2/2004	Fry	7,517,315	B2	4/2009	Willis
6,692,450	B1	2/2004	Coleman	7,530,356	B2	5/2009	Slayton
6,699,237	B2	3/2004	Weber	7,530,958	B2	5/2009	Slayton
6,716,184	B2	4/2004	Vaezy et al.	7,532,201	B2	5/2009	Quistgaard et al.
6,719,449	B1	4/2004	Laughlin	7,571,336	B2	8/2009	Barthe
6,719,694	B2	4/2004	Weng	7,601,120	B2	10/2009	Moilanen et al.
6,726,627	B1	4/2004	Lizzi et al.	7,615,015	B2	11/2009	Coleman
6,733,449	B1	5/2004	Krishnamurthy et al.	7,615,016	B2	11/2009	Barthe
6,749,624	B2	6/2004	Knowlton	7,652,411	B2	1/2010	Crunkilton et al.
6,772,490	B2	8/2004	Toda	7,662,114	B2	2/2010	Seip et al.
6,773,409	B2	8/2004	Truckai et al.	7,674,257	B2	3/2010	Pless et al.
6,775,404	B1	8/2004	Pagoulatos et al.	7,686,763	B2	3/2010	Vaezy et al.
6,790,187	B2	9/2004	Thompson et al.	7,713,203	B2	3/2010	Lacoste et al.
6,824,516	B2	11/2004	Batten et al.	7,694,406	B2	4/2010	Wildes et al.
6,825,176	B2	11/2004	White et al.	7,695,437	B2	4/2010	Quistgaard et al.
6,835,940	B2	12/2004	Morikawa et al.	7,727,156	B2	6/2010	Angelsen et al.
6,846,290	B2	1/2005	Lizzi et al.	7,758,524	B2	7/2010	Barthe
6,875,176	B2	4/2005	Mourad et al.	7,766,848	B2	8/2010	Desilets et al.
6,882,884	B1	4/2005	Mosk et al.	7,789,841	B2	9/2010	Huckle et al.
6,887,239	B2	5/2005	Elstrom	7,806,839	B2	10/2010	Mast et al.
6,889,089	B2	5/2005	Behl	7,815,570	B2	10/2010	Eshel et al.
6,896,657	B2	5/2005	Willis	7,819,826	B2	10/2010	Diederich et al.
6,902,536	B2	6/2005	Manna	7,828,734	B2	10/2010	Azhari et al.
6,905,466	B2	6/2005	Salgo	7,824,348	B2	11/2010	Barthe
6,918,907	B2	7/2005	Kelly	7,833,162	B2	11/2010	Hasegawa et al.
6,920,883	B2	7/2005	Besette	7,841,984	B2	11/2010	Cribbs et al.
6,921,371	B2	7/2005	Wilson	7,846,096	B2	12/2010	Mast et al.
6,932,771	B2	8/2005	Whitmore	7,857,773	B2	12/2010	Desilets et al.
6,932,814	B2	8/2005	Wood	7,875,023	B2	1/2011	Eshel et al.
6,936,044	B2	8/2005	McDaniel	7,901,359	B2	3/2011	Mandrusov et al.
6,936,046	B2	8/2005	Hissong	7,905,007	B2	3/2011	Calisti et al.
6,945,937	B2	9/2005	Culp et al.	7,905,844	B2	3/2011	Desilets et al.
6,948,843	B2	9/2005	Laugharn et al.	7,914,453	B2	3/2011	Slayton et al.
6,953,941	B2	10/2005	Nakano et al.	7,914,469	B2	3/2011	Torbati
6,958,043	B2	10/2005	Hissong	7,955,281	B2	6/2011	Pedersen et al.
6,971,994	B1	12/2005	Young et al.	7,967,764	B2	6/2011	Lidgren et al.
6,974,417	B2	12/2005	Lockwood	7,967,839	B2	6/2011	Flock et al.
6,976,492	B2	12/2005	Ingle	7,955,262	B2	7/2011	Rosenberg
6,992,305	B2	1/2006	Maezawa et al.	7,993,289	B2	8/2011	Quistgaard et al.
				8,057,465	B2	9/2011	Sliwa, Jr. et al.
				8,057,389	B2	11/2011	Barthe et al.
				8,066,641	B2	11/2011	Barthe et al.
				8,123,707	B2	2/2012	Huckle et al.

(56)

References Cited

U.S. PATENT DOCUMENTS

8,128,618 B2	3/2012	Gliklich et al.	9,114,247 B2	8/2015	Barthe et al.
8,133,180 B2	3/2012	Slayton et al.	9,180,314 B2	11/2015	Desilets et al.
8,133,191 B2	3/2012	Rosenberg et al.	9,216,276 B2	12/2015	Slayton et al.
8,142,200 B2	3/2012	Crunkilton et al.	9,220,915 B2	12/2015	Liu et al.
8,152,904 B2	4/2012	Slobodzian et al.	9,272,162 B2	3/2016	Slayton et al.
8,162,858 B2	4/2012	Manna et al.	9,283,409 B2	3/2016	Slayton et al.
8,166,332 B2	4/2012	Barthe et al.	9,283,410 B2	3/2016	Slayton et al.
8,182,428 B2	5/2012	Angelsen et al.	9,295,607 B2	3/2016	Rosenberg
8,197,409 B2	6/2012	Foley et al.	9,308,390 B2	4/2016	Youngquist
8,206,299 B2	6/2012	Foley et al.	9,308,391 B2	4/2016	Liu et al.
8,208,346 B2	6/2012	Crunkilton	9,314,650 B2	4/2016	Rosenberg et al.
8,211,017 B2	7/2012	Foley et al.	9,320,537 B2	4/2016	Slayton et al.
8,262,591 B2	9/2012	Pedersen et al.	9,345,910 B2	5/2016	Slayton et al.
8,262,650 B2	9/2012	Zanelli et al.	9,421,029 B2	8/2016	Barthe et al.
8,264,126 B2	9/2012	Toda et al.	9,427,600 B2	8/2016	Barthe et al.
8,273,037 B2	9/2012	Kreindel et al.	9,427,601 B2	8/2016	Barthe et al.
8,282,554 B2	10/2012	Makin et al.	9,433,803 B2	9/2016	Lin et al.
8,292,835 B1	10/2012	Cimino	9,440,093 B2	9/2016	Homer
8,298,163 B1	10/2012	Cimino	9,440,096 B2	9/2016	Barthe et al.
8,333,700 B1	12/2012	Barthe et al.	9,492,645 B2	11/2016	Zhou et al.
8,334,637 B2	12/2012	Crunkilton et al.	9,492,686 B2	11/2016	Da Silva
8,337,407 B2	12/2012	Quistgaard et al.	9,498,651 B2	11/2016	Sapozhnikov et al.
8,343,051 B2	1/2013	Desilets et al.	9,510,802 B2	12/2016	Barthe et al.
8,454,540 B2	1/2013	Eshel et al.	9,522,290 B2	12/2016	Slayton et al.
8,366,622 B2	2/2013	Slayton et al.	9,532,832 B2	1/2017	Ron Edoute et al.
8,398,549 B2	3/2013	Palmeri et al.	9,533,174 B2	1/2017	Barthe et al.
8,409,097 B2	4/2013	Slayton et al.	9,533,175 B2	1/2017	Slayton et al.
8,425,435 B2	4/2013	Wing et al.	9,545,529 B2	1/2017	Britva et al.
8,388,535 B2	5/2013	Weng et al.	9,566,454 B2	2/2017	Barthe et al.
8,444,562 B2	5/2013	Barthe et al.	9,623,267 B2	4/2017	Ulric et al.
8,460,193 B2	6/2013	Barthe et al.	9,694,211 B2	7/2017	Barthe et al.
8,480,585 B2	7/2013	Slayton et al.	9,694,212 B2	7/2017	Barthe et al.
8,486,001 B2	7/2013	Weyant	9,700,340 B2	7/2017	Barthe et al.
8,506,486 B2	8/2013	Slayton et al.	9,707,412 B2	7/2017	Slayton et al.
8,512,250 B2	8/2013	Quistgaard et al.	9,710,607 B2	7/2017	Ramdas et al.
8,523,775 B2	9/2013	Barthe et al.	9,713,731 B2	7/2017	Slayton et al.
8,523,849 B2	9/2013	Liu et al.	9,802,063 B2	10/2017	Barthe et al.
8,535,228 B2	9/2013	Slayton et al.	9,827,449 B2	11/2017	Barthe et al.
8,570,837 B2	10/2013	Toda et al.	9,827,450 B2	11/2017	Slayton et al.
8,573,392 B2	11/2013	Bennett et al.	9,833,639 B2	12/2017	Slayton et al.
8,583,211 B2	11/2013	Salomir et al.	9,833,640 B2	12/2017	Barthe et al.
8,585,618 B2	11/2013	Hunziker et al.	9,895,560 B2	2/2018	Barthe et al.
8,604,672 B2	12/2013	Toda et al.	9,907,535 B2	3/2018	Barthe et al.
8,622,937 B2	1/2014	Weng et al.	9,919,167 B2	3/2018	Domankevitz
8,636,665 B2	1/2014	Slayton et al.	9,974,982 B2	5/2018	Slayton et al.
8,641,622 B2	2/2014	Barthe et al.	1,001,072 A1	7/2018	Slayton et al.
8,663,112 B2	3/2014	Slayton et al.	1,004,618 A1	8/2018	Barthe et al.
8,672,848 B2	3/2014	Slayton et al.	2001/0009997 A1	7/2001	Pope
8,690,778 B2	4/2014	Slayton et al.	2001/0009999 A1	7/2001	Kaufman et al.
8,690,779 B2	4/2014	Slayton et al.	2001/0014780 A1	8/2001	Martin
8,690,780 B2	4/2014	Slayton et al.	2001/0014819 A1	8/2001	Ingle
8,708,935 B2	4/2014	Barthe et al.	2001/0031922 A1*	10/2001	Weng A61B 17/0057 600/439
8,715,186 B2	5/2014	Slayton et al.	2001/0039380 A1	11/2001	Larson et al.
8,726,781 B2	5/2014	Eckhoff et al.	2001/0041880 A1	11/2001	Briskken
8,728,071 B2	5/2014	Lischinsky et al.	2002/0000763 A1	1/2002	Jones
8,753,295 B2	6/2014	Thierman	2002/0002345 A1	1/2002	Marlinghaus
8,758,253 B2	6/2014	Sano et al.	2002/0040199 A1	4/2002	Klopotek
8,836,203 B2	9/2014	Nobles et al.	2002/0040442 A1	4/2002	Ishidera
8,857,438 B2	10/2014	Barthe et al.	2002/0055702 A1	5/2002	Atala
8,858,471 B2	10/2014	Barthe et al.	2002/0062077 A1	5/2002	Emmenegger
8,915,853 B2	12/2014	Barthe et al.	2002/0062142 A1	5/2002	Knowlton
8,915,854 B2	12/2014	Slayton et al.	2002/0072691 A1	6/2002	Thompson et al.
8,915,870 B2	12/2014	Barthe et al.	2002/0082528 A1	6/2002	Friedman
8,920,320 B2	12/2014	Stecco et al.	2002/0082529 A1	6/2002	Suorsa et al.
8,920,324 B2	12/2014	Slayton et al.	2002/0082589 A1	6/2002	Friedman
8,926,533 B2	1/2015	Bockenstedt et al.	2002/0087080 A1	7/2002	Slayton
8,932,224 B2	1/2015	Barthe et al.	2002/0095143 A1	7/2002	Key
8,932,238 B2	1/2015	Wing et al.	2002/0099094 A1	7/2002	Anderson
8,968,205 B2	3/2015	Zeng et al.	2002/0115917 A1	8/2002	Honda et al.
9,011,336 B2	4/2015	Slayton et al.	2002/0128639 A1	8/2002	Pless et al.
9,039,617 B2	5/2015	Slayton et al.	2002/0128648 A1	9/2002	Weber
9,039,619 B2	5/2015	Barthe et al.	2002/0143252 A1	10/2002	Dunne et al.
9,050,116 B2	6/2015	Homer	2002/0156400 A1	10/2002	Babaev
9,095,697 B2	8/2015	Barthe et al.	2002/0161357 A1	10/2002	Anderson
9,107,798 B2	8/2015	Azhari et al.	2002/0165529 A1	11/2002	Danek
			2002/0168049 A1	11/2002	Schriever
			2002/0169394 A1	11/2002	Eppstein et al.
			2002/0169442 A1	11/2002	Neev

(56)

References Cited

U.S. PATENT DOCUMENTS

2002/0173721 A1	11/2002	Grunwald et al.	2004/0105559 A1	6/2004	Aylward et al.
2002/0193784 A1	12/2002	McHale et al.	2004/0106867 A1	6/2004	Eshel et al.
2002/0193831 A1	12/2002	Smith	2004/0122323 A1	6/2004	Vortman et al.
2003/0009153 A1	1/2003	Briskin et al.	2004/0122493 A1	6/2004	Ishibashi et al.
2003/0014039 A1	1/2003	Barzell et al.	2004/0143297 A1	7/2004	Ramsey
2003/0018255 A1	1/2003	Martin	2004/0152982 A1	8/2004	Hwang et al.
2003/0018270 A1	1/2003	Makin et al.	2004/0158150 A1	8/2004	Rabiner et al.
2003/0023283 A1*	1/2003	McDaniel A61K 8/02 607/88	2004/0186535 A1	9/2004	Knowlton
2003/0028111 A1	2/2003	Vaezy et al.	2004/0189155 A1	9/2004	Funakubo
2003/0028113 A1	2/2003	Gilbert et al.	2004/0206365 A1	10/2004	Knowlton
2003/0032900 A1	2/2003	Ella	2004/0210214 A1	10/2004	Knowlton
2003/0036706 A1	2/2003	Slayton et al.	2004/0217675 A1	11/2004	Desilets
2003/0040739 A1	2/2003	Koop	2004/0249318 A1	12/2004	Tanaka
2003/0050678 A1	3/2003	Sierra	2004/0254620 A1	12/2004	Lacoste
2003/0055308 A1	3/2003	Friemel et al.	2004/0267252 A1	12/2004	Washington et al.
2003/0055417 A1	3/2003	Truckai et al.	2005/0033201 A1	2/2005	Takahashi
2003/0060736 A1	3/2003	Martin et al.	2005/0033316 A1	2/2005	Kertz
2003/0065313 A1	4/2003	Koop	2005/0038340 A1	2/2005	Vaezy et al.
2003/0066708 A1	4/2003	Allison et al.	2005/0055018 A1	3/2005	Kreindel
2003/0073907 A1	4/2003	Taylor	2005/0055073 A1	3/2005	Weber
2003/0074023 A1	4/2003	Kaplan	2005/0061834 A1	3/2005	Garcia et al.
2003/0083536 A1	5/2003	Eshel	2005/0070961 A1	3/2005	Maki
2003/0092988 A1	5/2003	Makin	2005/0074407 A1	4/2005	Smith
2003/0097071 A1	5/2003	Halmann et al.	2005/0080469 A1	4/2005	Larson
2003/0099383 A1	5/2003	Lefebvre	2005/0085731 A1	4/2005	Miller et al.
2003/0125629 A1	7/2003	Ustuner	2005/0091770 A1	5/2005	Mourad et al.
2003/0135135 A1	7/2003	Miwa et al.	2005/0096542 A1	5/2005	Weng et al.
2003/0139790 A1	7/2003	Ingle et al.	2005/0104690 A1	5/2005	Larson et al.
2003/0149366 A1	8/2003	Stringer et al.	2005/0113689 A1	5/2005	Gritzky
2003/0153961 A1	8/2003	Babaev	2005/0131302 A1	6/2005	Poland
2003/0171678 A1	9/2003	Batten et al.	2005/0137656 A1	6/2005	Malak
2003/0171701 A1	9/2003	Babaev	2005/0143677 A1	6/2005	Young et al.
2003/0176790 A1	9/2003	Slayton	2005/0154313 A1	7/2005	Desilets
2003/0191396 A1	10/2003	Sanghvi	2005/0154314 A1	7/2005	Quistgaard
2003/0199794 A1	10/2003	Sakurai et al.	2005/0154332 A1	7/2005	Zanelli
2003/0200481 A1	10/2003	Stanley	2005/0154431 A1	7/2005	Quistgaard
2003/0212129 A1	11/2003	Liu et al.	2005/0187495 A1	8/2005	Quistgaard
2003/0212351 A1	11/2003	Hissong	2005/0191252 A1	9/2005	Mitsui
2003/0212393 A1	11/2003	Knowlton	2005/0193451 A1	9/2005	Quistgaard
2003/0216648 A1	11/2003	Lizzi et al.	2005/0193820 A1	9/2005	Sheljaskow et al.
2003/0216795 A1	11/2003	Harth	2005/0197681 A1	9/2005	Barolet et al.
2003/0220536 A1	11/2003	Hissong	2005/0228281 A1	10/2005	Nefos
2003/0220585 A1	11/2003	Hissong	2005/0240127 A1	10/2005	Seip et al.
2003/0229331 A1	12/2003	Briskin et al.	2005/0240170 A1	10/2005	Zhang et al.
2003/0233085 A1	12/2003	Giammarusti	2005/0251120 A1	11/2005	Anderson et al.
2003/0236487 A1	12/2003	Knowlton	2005/0251125 A1	11/2005	Pless et al.
2004/0000316 A1	1/2004	Knowlton	2005/0256406 A1	11/2005	Barthe
2004/0001809 A1	1/2004	Briskin	2005/0261584 A1	11/2005	Eshel
2004/0002658 A1	1/2004	Marian, Jr.	2005/0261585 A1	11/2005	Makin et al.
2004/0002705 A1	1/2004	Knowlton	2005/0267454 A1	12/2005	Hissong
2004/0010222 A1	1/2004	Nunomura et al.	2005/0288748 A1	12/2005	Li et al.
2004/0015079 A1	1/2004	Berger et al.	2006/0004306 A1	1/2006	Altshuler
2004/0015106 A1	1/2004	Coleman	2006/0020260 A1	1/2006	Dover et al.
2004/0030227 A1	2/2004	Littrup	2006/0025756 A1	2/2006	Francischelli
2004/0030268 A1	2/2004	Weng et al.	2006/0042201 A1	3/2006	Curry
2004/0039312 A1	2/2004	Hillstead	2006/0058664 A1	3/2006	Barthe
2004/0039418 A1	2/2004	Elstrom	2006/0058671 A1	3/2006	Vitek et al.
2004/0041563 A1	3/2004	Lewin et al.	2006/0058707 A1	3/2006	Barthe
2004/0041880 A1	3/2004	Ikeda et al.	2006/0058712 A1	3/2006	Altshuler et al.
2004/0042168 A1	3/2004	Yang et al.	2006/0074309 A1	4/2006	Bonnefous
2004/0044375 A1	3/2004	Diederich et al.	2006/0074313 A1	4/2006	Slayton et al.
2004/0049134 A1	3/2004	Tosaya et al.	2006/0074314 A1	4/2006	Slayton
2004/0049734 A1	3/2004	Tosaya et al.	2006/0074355 A1	4/2006	Slayton
2004/0059266 A1	3/2004	Fry	2006/0079816 A1	4/2006	Barthe
2004/0068186 A1	4/2004	Ishida et al.	2006/0079868 A1	4/2006	Makin
2004/0073079 A1	4/2004	Altshuler et al.	2006/0084891 A1	4/2006	Barthe
2004/0073113 A1	4/2004	Salgo	2006/0089632 A1	4/2006	Barthe
2004/0073115 A1	4/2004	Horzewski et al.	2006/0089688 A1	4/2006	Panescu
2004/0073116 A1	4/2004	Smith	2006/0094988 A1	5/2006	Tosaya
2004/0073204 A1	4/2004	Ryan et al.	2006/0111744 A1	5/2006	Makin
2004/0077977 A1	4/2004	Ella et al.	2006/0116583 A1	6/2006	Ogasawara et al.
2004/0082857 A1	4/2004	Schonenberger	2006/0116671 A1	6/2006	Slayton
2004/0082859 A1	4/2004	Schaer	2006/0122508 A1	6/2006	Slayton
2004/0102697 A1	5/2004	Evron	2006/0122509 A1	6/2006	Desilets
			2006/0161062 A1	7/2006	Arditi et al.
			2006/0184069 A1	8/2006	Vaitekunas
			2006/0184071 A1	8/2006	Klopotek
			2006/0189972 A1	8/2006	Grossman
			2006/0206105 A1	9/2006	Chopra

(56)

References Cited

U.S. PATENT DOCUMENTS

2006/0224090 A1	10/2006	Ostrovsky et al.	2009/0171252 A1	7/2009	Bockenstedt et al.
2006/0229514 A1	10/2006	Wiener	2009/0177122 A1	7/2009	Peterson
2006/0241440 A1	10/2006	Eshel	2009/0177123 A1	7/2009	Peterson
2006/0241442 A1	10/2006	Barthe	2009/0182231 A1	7/2009	Barthe et al.
2006/0241470 A1	10/2006	Novak et al.	2009/0198157 A1	8/2009	Babaev et al.
2006/0241576 A1	10/2006	Diederich et al.	2009/0216159 A1	8/2009	Slayton et al.
2006/0250046 A1	11/2006	Koizumi et al.	2009/0226424 A1	9/2009	Hsu
2006/0282691 A1	12/2006	Barthe	2009/0227910 A1	9/2009	Pedersen et al.
2006/0291710 A1	12/2006	Wang et al.	2009/0230823 A1	9/2009	Kushculey et al.
2007/0016039 A1	1/2007	Vortman et al.	2009/0253988 A1	10/2009	Slayton et al.
2007/0032784 A1	2/2007	Gliklich et al.	2009/0281463 A1	11/2009	Chapelon et al.
2007/0035201 A1	2/2007	Desilets	2009/0312693 A1	12/2009	Thapliyal et al.
2007/0055154 A1	3/2007	Torbati	2009/0318909 A1	12/2009	Debenedictis et al.
2007/0055155 A1	3/2007	Owen et al.	2009/0326420 A1	12/2009	Moonen et al.
2007/0055156 A1	3/2007	Desilets et al.	2010/0011236 A1	1/2010	Barthe et al.
2007/0065420 A1	3/2007	Johnson	2010/0022919 A1	1/2010	Peterson
2007/0083120 A1	4/2007	Cain et al.	2010/0022921 A1	1/2010	Seip et al.
2007/0087060 A1	4/2007	Dietrich	2010/0022922 A1	1/2010	Barthe et al.
2007/0088245 A1	4/2007	Babaev et al.	2010/0030076 A1	2/2010	Vortman et al.
2007/0088346 A1	4/2007	Mirizzi et al.	2010/0042020 A1	2/2010	Ben-Ezra
2007/0161902 A1	7/2007	Dan	2010/0049178 A1	2/2010	Deem et al.
2007/0166357 A1	7/2007	Shaffer et al.	2010/0056925 A1	3/2010	Zhang et al.
2007/0167709 A1	7/2007	Slayton	2010/0100014 A1	4/2010	Eshel et al.
2007/0208253 A1	9/2007	Slayton	2010/0113983 A1	5/2010	Heckerman et al.
2007/0219604 A1	9/2007	Yaroslavsky et al.	2010/0130891 A1	5/2010	Taggart et al.
2007/0219605 A1	9/2007	Yaroslavsky et al.	2010/0160782 A1	6/2010	Slayton et al.
2007/0238994 A1	10/2007	Stecco et al.	2010/0160837 A1	6/2010	Hunziker et al.
2007/0239075 A1	10/2007	Rosenberg	2010/0168576 A1	7/2010	Poland et al.
2007/0239077 A1	10/2007	Azhari et al.	2010/0191120 A1	7/2010	Kraus et al.
2007/0239079 A1	10/2007	Manstein et al.	2010/0241035 A1	9/2010	Barthe et al.
2007/0239142 A1	10/2007	Altshuler	2010/0249602 A1	9/2010	Buckley et al.
2008/0015435 A1	1/2008	Cribbs et al.	2010/0249669 A1	9/2010	Ulric et al.
2008/0027328 A1	1/2008	Klopotek	2010/0256489 A1	10/2010	Pedersen et al.
2008/0033458 A1	2/2008	McLean et al.	2010/0274161 A1	10/2010	Azhari et al.
2008/0039724 A1	2/2008	Seip et al.	2010/0280420 A1	11/2010	Barthe et al.
2008/0071255 A1	3/2008	Barthe	2010/0286518 A1	11/2010	Lee et al.
2008/0086054 A1	4/2008	Slayton	2010/0312150 A1	12/2010	Douglas et al.
2008/0086056 A1	4/2008	Chang et al.	2011/0040171 A1	2/2011	Foley et al.
2008/0097214 A1	4/2008	Meyers et al.	2011/0040190 A1	2/2011	Jahnke et al.
2008/0097253 A1	4/2008	Pedersen et al.	2011/0040213 A1	2/2011	Dietz et al.
2008/0114251 A1	5/2008	Weymer et al.	2011/0040214 A1	2/2011	Foley et al.
2008/0139943 A1	6/2008	Deng et al.	2011/0066084 A1	3/2011	Desilets et al.
2008/0139974 A1	6/2008	Da Silva	2011/0077514 A1	3/2011	Ulric et al.
2008/0146970 A1	6/2008	Litman et al.	2011/0087099 A1	4/2011	Eshel et al.
2008/0167556 A1	7/2008	Thompson	2011/0087255 A1	4/2011	McCormack et al.
2008/0183077 A1	7/2008	Moreau-Gobard et al.	2011/0112405 A1	5/2011	Barthe et al.
2008/0183110 A1	7/2008	Davenport et al.	2011/0144490 A1	6/2011	Davis et al.
2008/0188745 A1	8/2008	Chen et al.	2011/0178444 A1	7/2011	Slayton et al.
2008/0194964 A1	8/2008	Randall et al.	2011/0178541 A1	7/2011	Azhari
2008/0195000 A1	8/2008	Spooner et al.	2011/0190745 A1	8/2011	Uebelhoer et al.
2008/0200810 A1	8/2008	Buchalter	2011/0201976 A1	8/2011	Sanghvi et al.
2008/0200813 A1	8/2008	Quistgaard	2011/0251524 A1	10/2011	Azhari et al.
2008/0214966 A1	9/2008	Slayton	2011/0251527 A1	10/2011	Kushculey et al.
2008/0214988 A1	9/2008	Altshuler et al.	2011/0270137 A1	11/2011	Goren et al.
2008/0221491 A1	9/2008	Slayton	2011/0319793 A1	12/2011	Henrik et al.
2008/0223379 A1	9/2008	Stuker et al.	2011/0319794 A1	12/2011	Gertner
2008/0242991 A1	10/2008	Moon et al.	2012/0004549 A1	1/2012	Barthe et al.
2008/0243035 A1	10/2008	Crunkilton	2012/0016239 A1	1/2012	Barthe et al.
2008/0269608 A1	10/2008	Anderson et al.	2012/0029353 A1	2/2012	Slayton et al.
2008/0275342 A1	11/2008	Barthe	2012/0035473 A1	2/2012	Sanghvi et al.
2008/0281206 A1	11/2008	Bartlett et al.	2012/0035475 A1	2/2012	Barthe et al.
2008/0281236 A1	11/2008	Eshel et al.	2012/0035476 A1	2/2012	Barthe et al.
2008/0281237 A1	11/2008	Slayton	2012/0046547 A1	2/2012	Barthe et al.
2008/0281255 A1	11/2008	Slayton	2012/0053458 A1	3/2012	Barthe et al.
2008/0294073 A1	11/2008	Barthe	2012/0059288 A1	3/2012	Barthe et al.
2008/0319356 A1	12/2008	Cain	2012/0111339 A1	5/2012	Barthe et al.
2009/0005680 A1	1/2009	Jones et al.	2012/0123304 A1	5/2012	Rybyanets et al.
2009/0012394 A1	1/2009	Hobelsberger et al.	2012/0136280 A1	5/2012	Rosenberg et al.
2009/0043198 A1	2/2009	Milner et al.	2012/0136282 A1	5/2012	Rosenberg et al.
2009/0043293 A1	2/2009	Pankratov et al.	2012/0143056 A1	6/2012	Slayton et al.
2009/0048514 A1	2/2009	Azhari et al.	2012/0143100 A1	6/2012	Jeong et al.
2009/0069677 A1	3/2009	Chen et al.	2012/0165668 A1	6/2012	Slayton et al.
2009/0093737 A1	4/2009	Chomas et al.	2012/0165848 A1	6/2012	Slayton et al.
2009/0156969 A1	6/2009	Santangelo	2012/0191019 A1	7/2012	Desilets et al.
2009/0163807 A1	6/2009	Sliwa	2012/0191020 A1	7/2012	Vitek et al.
			2012/0197120 A1	8/2012	Makin et al.
			2012/0197121 A1	8/2012	Slayton et al.
			2012/0209150 A1	8/2012	Zeng et al.
			2012/0215105 A1	8/2012	Slayton et al.

(56)

References Cited

U.S. PATENT DOCUMENTS

2012/0271202 A1 10/2012 Wisdom
 2012/0271294 A1 10/2012 Barthe et al.
 2012/0296240 A1 11/2012 Azhari et al.
 2012/0302883 A1 11/2012 Kong et al.
 2012/0316426 A1 12/2012 Foley et al.
 2012/0330197 A1 12/2012 Makin et al.
 2012/0330222 A1 12/2012 Makin et al.
 2012/0330223 A1 12/2012 Makin et al.
 2012/0330283 A1 12/2012 Hyde et al.
 2012/0330284 A1 12/2012 Hyde et al.
 2013/0012755 A1 1/2013 Slayton
 2013/0012816 A1 1/2013 Slayton et al.
 2013/0012838 A1 1/2013 Jaeger et al.
 2013/0012842 A1 1/2013 Barthe
 2013/0018285 A1 1/2013 Park et al.
 2013/0018286 A1 1/2013 Slayton et al.
 2013/0046209 A1 2/2013 Slayton et al.
 2013/0051178 A1 2/2013 Rybyanets
 2013/0060170 A1 3/2013 Lee et al.
 2013/0066208 A1 3/2013 Barthe et al.
 2013/0066237 A1 3/2013 Smotrich et al.
 2013/0072826 A1 3/2013 Slayton et al.
 2013/0073001 A1 3/2013 Campbell
 2013/0096471 A1 4/2013 Slayton et al.
 2013/0190659 A1 7/2013 Slayton et al.
 2013/0211293 A1 8/2013 Auboiroux et al.
 2013/0225994 A1 8/2013 Hsu et al.
 2013/0268032 A1 10/2013 Neev
 2013/0274603 A1 10/2013 Barthe et al.
 2013/0281853 A1 10/2013 Slayton et al.
 2013/0281891 A1 10/2013 Slayton et al.
 2013/0296697 A1 11/2013 Slayton et al.
 2013/0296700 A1 11/2013 Slayton et al.
 2013/0296743 A1 11/2013 Lee et al.
 2013/0303904 A1 11/2013 Barthe et al.
 2013/0303905 A1 11/2013 Barthe et al.
 2013/0310714 A1 11/2013 Eshel et al.
 2013/0310863 A1 11/2013 Makin et al.
 2013/0345562 A1 12/2013 Barthe et al.
 2014/0024974 A1 1/2014 Slayton et al.
 2014/0050054 A1 2/2014 Toda et al.
 2014/0081300 A1 3/2014 Melodelima et al.
 2014/0082907 A1 3/2014 Barthe et al.
 2014/0117814 A1 5/2014 Toda et al.
 2014/0142430 A1 5/2014 Slayton et al.
 2014/0148834 A1 5/2014 Barthe et al.
 2014/0180174 A1 6/2014 Slayton et al.
 2014/0187944 A1 7/2014 Slayton et al.
 2014/0188015 A1 7/2014 Slayton et al.
 2014/0188145 A1 7/2014 Slayton et al.
 2014/0194723 A1 7/2014 Herzog et al.
 2014/0208856 A1 7/2014 Schmid
 2014/0221823 A1 8/2014 Keogh et al.
 2014/0236049 A1 8/2014 Barthe et al.
 2014/0236061 A1 8/2014 Lee et al.
 2014/0243713 A1 8/2014 Slayton et al.
 2014/0257145 A1 9/2014 Emery
 2014/0276055 A1 9/2014 Barthe et al.
 2015/0000674 A1 1/2015 Barthe et al.
 2015/0025420 A1 1/2015 Slayton et al.
 2015/0080723 A1 3/2015 Barthe et al.
 2015/0080771 A1 3/2015 Barthe et al.
 2015/0080874 A1 3/2015 Slayton et al.
 2015/0088182 A1 3/2015 Slayton et al.
 2015/0141734 A1 5/2015 Chapelon et al.
 2015/0164734 A1 6/2015 Slayton et al.
 2015/0165238 A1 6/2015 Slayton et al.
 2015/0165243 A1 6/2015 Slayton et al.
 2015/0174388 A1 6/2015 Slayton
 2015/0202468 A1 7/2015 Slayton et al.
 2015/0217141 A1 8/2015 Barthe et al.
 2015/0238258 A1 8/2015 Palero et al.
 2015/0321026 A1 11/2015 Branson et al.
 2015/0360058 A1 12/2015 Barthe et al.
 2015/0374333 A1 12/2015 Barthe et al.

2015/0375014 A1 12/2015 Slayton et al.
 2016/0001097 A1 1/2016 Cho et al.
 2016/0016015 A1 1/2016 Slayton et al.
 2016/0027994 A1 1/2016 Toda et al.
 2016/0151618 A1 6/2016 Powers et al.
 2016/0175619 A1 6/2016 Lee et al.
 2016/0206335 A1 7/2016 Slayton
 2016/0206341 A1 7/2016 Slayton
 2016/0256675 A1 9/2016 Slayton
 2016/0296769 A1 10/2016 Barthe et al.
 2016/0361571 A1 12/2016 Bernabei
 2016/0361572 A1 12/2016 Slayton
 2017/0028227 A1 2/2017 Emery et al.
 2017/0043190 A1 2/2017 Barthe et al.
 2017/0050019 A1 2/2017 Ron Edoute et al.
 2017/0080257 A1 3/2017 Paunescu et al.
 2017/0100585 A1 4/2017 Hall et al.
 2017/0136263 A1 5/2017 Reil
 2017/0209201 A1 7/2017 Slayton et al.
 2017/0304654 A1 10/2017 Blanche et al.
 2018/0001113 A1 1/2018 Streeter
 2018/0015308 A1 1/2018 Reed et al.
 2018/0043147 A1 2/2018 Slayton
 2018/0099162 A1 4/2018 Bernabei
 2018/0099163 A1 4/2018 Bernabei
 2018/0272156 A1 9/2018 Slayton et al.
 2018/0272158 A1 9/2018 Barthe et al.
 2018/0272159 A1 9/2018 Slayton et al.

FOREIGN PATENT DOCUMENTS

DE 10140064 3/2003
 DE 10219297 11/2003
 DE 10219217 12/2004
 DE 20314479 12/2004
 EP 0142215 5/1984
 EP 0344773 12/1989
 EP 1479412 11/1991
 EP 0473553 4/1992
 EP 670147 2/1995
 EP 0661029 7/1995
 EP 724894 2/1996
 EP 763371 11/1996
 EP 1044038 10/2000
 EP 1050322 11/2000
 EP 1234566 8/2002
 EP 1262160 12/2002
 EP 0659387 4/2003
 EP 1374944 1/2004
 EP 1028660 1/2008
 EP 1874241 1/2008
 EP 1362223 5/2008
 EP 1750804 7/2008
 EP 1283690 11/2008
 EP 1811901 4/2009
 EP 1785164 8/2009
 EP 2230904 9/2010
 EP 1501331 6/2011
 EP 2066405 11/2011
 EP 2474050 7/2012
 EP 2709726 11/2015
 EP 1538980 1/2017
 EP 2897547 11/2017
 FR 2532851 9/1983
 FR 2685872 1/1992
 FR 2672486 8/1992
 FR 2703254 3/1994
 GB 2113099 8/1983
 IL 102516 1/1996
 IL 112369 8/1999
 IL 120079 3/2001
 JP 63036171 2/1988
 JP 03048299 3/1991
 JP 3123559 5/1991
 JP 03136642 6/1991
 JP 4089058 3/1992
 JP 04150847 5/1992
 JP 7080087 3/1995
 JP 07505793 6/1995

(56) References Cited

FOREIGN PATENT DOCUMENTS

JP	7184907	7/1995
JP	7222782	8/1995
JP	09047458	2/1997
JP	9108288	4/1997
JP	9503926	4/1997
JP	11123226	5/1999
JP	11505440	5/1999
JP	11506636	6/1999
JP	10248850	9/1999
JP	2000126310	5/2000
JP	2000166940	6/2000
JP	2000233009	8/2000
JP	2001170068	6/2001
JP	2002505596	2/2002
JP	2002078764	3/2002
JP	2002515786	5/2002
JP	2002521118	7/2002
JP	2002537939	11/2002
JP	2003050298	7/2003
JP	2003204982	7/2003
JP	2004-504898	2/2004
JP	2004-507280	3/2004
JP	2004-509671	4/2004
JP	2004-512856	4/2004
JP	2004147719	5/2004
JP	2005503388	2/2005
JP	2005527336	9/2005
JP	2005323213	11/2005
JP	2006520247	9/2006
JP	2008515559	5/2008
JP	2009518126	5/2009
JP	2010517695	5/2010
KR	1020010024871	3/2001
KR	100400870	10/2003
KR	20060121267	11/2006
KR	1020060113930	11/2006
KR	1020070065332	6/2007
KR	1020070070161	7/2007
KR	1020070098856	10/2007
KR	1020070104878	10/2007
KR	1020070114105	11/2007
KR	1020000059516	4/2012
KR	10-2013-0124598	11/2013
KR	10-1365946	2/2014
TW	386883	9/2000
TW	201208734 A	3/2012
WO	WO9312742	7/1993
WO	WO9524159	9/1995
WO	WO9625888	8/1996
WO	WO9634568	11/1996
WO	WO9639079	12/1996
WO	WO9735518	10/1997
WO	WO9832379	7/1998
WO	WO9852465	11/1998
WO	WO9933520	7/1999
WO	WO9949788	10/1999
WO	WO200006032	2/2000
WO	WO0015300	3/2000
WO	WO0021612	4/2000
WO	WO0053113	9/2000
WO	WO0128623	4/2001
WO	WO01045550	6/2001
WO	WO0182777	11/2001
WO	WO0182778	11/2001
WO	WO0187161	11/2001
WO	WO01080709	11/2001
WO	WO2001087161	11/2001
WO	WO0209812	2/2002
WO	WO0209813	2/2002
WO	WO02015768	2/2002
WO	WO0224050	3/2002
WO	WO2002054018	7/2002
WO	WO02092168	11/2002
WO	WO03053266	7/2003
WO	WO03065347	8/2003

WO	WO03070105	8/2003
WO	WO03077833	9/2003
WO	WO03086215	10/2003
WO	WO03096883	11/2003
WO	WO03099177	12/2003
WO	WO03099382	12/2003
WO	WO03101530	12/2003
WO	WO2004000116	12/2003
WO	WO2004080147	9/2004
WO	WO2004110558	12/2004
WO	WO2005/011804	2/2005
WO	WO2005065408	7/2005
WO	WO2005065409	7/2005
WO	WO2005090978	9/2005
WO	WO2005113068	12/2005
WO	WO2006/042163	4/2006
WO	WO2006036870	4/2006
WO	WO2006042168	4/2006
WO	WO2006042201	4/2006
WO	WO2006065671	6/2006
WO	WO2006082573	8/2006
WO	WO2006104568	10/2006
WO	WO2007067563	6/2007
WO	WO2008036479	3/2008
WO	WO2008036622	3/2008
WO	WO2008144274	11/2008
WO	WO2009013729	1/2009
WO	WO2009149390	10/2009
WO	WO2012134645	10/2012
WO	WO2013048912	4/2013
WO	WO2013178830	12/2013
WO	WO2014045216	3/2014
WO	WO2014055708	4/2014
WO	WO2014057388	4/2014
WO	WO2014127091	8/2014
WO	WO2015160708	10/2015
WO	WO2016054155	4/2016
WO	WO2017127328	7/2017
WO	WO2017149506	9/2017
WO	WO2017165595	9/2017
WO	WO2017212489	12/2017
WO	WO2018035012	2/2018

OTHER PUBLICATIONS

Federal Circuit Order Granting Ulthera Motion to Remand, re: 2018-1542; 4 pages [022] (Dated May 25, 2018).

Agren, Magnus S. et al., Collagenase in Wound Healing: Effect of Wound Age and Type. The Journal of Investigative Dermatology, vol. 99/No. 6, (Dec. 1992).

Alam, M., "The future of noninvasive procedural dermatology". Semin Cutan Med Surg. Mar. 2013; 32(1):59-61.

Alam, M., et al., "Ultrasound tightening of facial and neck skin: a rater-blinded prospective cohort study". J Am Acad Dermatol. 2010. 62(2): p. 262-9.

Alexiades-Armenakas, M., "Ultrasound Technologies for Dermatologic Techniques". J Drugs Derm. 2014. 12 (11): p. 1305.

Alster, T.S., et. al., "Noninvasive lifting of arm, thigh, and knee skin with transcutaneous intense focused ultrasound". Dermatol Surg. 2012. 38(5): p. 754-9.

Alster, Tinas S., Tanzi, Elizabeth L., "Cellulite Treatment using a Novel Combination Radiofrequency, Infrared Light, and Mechanical Tissue Manipulation Device," Journal of Cosmetic & Laser Therapy, Jun. 2005, vol. 7, Issue 2, pp. 81-85.

Arosarena, O., "Options and Challenges for Facial Rejuvenation in Patients With Higher Fitzpatrick Skin Phototypes". JAMA Facial Plastic Surgery, 2015.

Arthur et al., "Non-invasive estimation of hyperthermia temperatures with ultrasound," Int. J. Hyperthermia, Sep. 2005, 21(6), pp. 589-600.

Barthe et al., "Ultrasound therapy system and ablation results utilizing miniature imaging/therapy arrays," Ultrasonics Symposium, 2004 IEEE, Aug. 23, 2004, pp. 1792-1795, vol. 3.

Bozec, Laurent et al., Thermal Denaturation Studies of Collagen by Microthermal Analysis and Atomic Force Microscopy, Biophysical Journal, vol. 101, pp. 228-236. (Jul. 2001).

(56)

References Cited

OTHER PUBLICATIONS

- Brobst, R.W., et. al., "Noninvasive Treatment of the Neck". *Facial Plast Surg Clin North Am*, 2014. 22(2): p. 191-202.
- Brobst, R.W., et., al., "Ulthera: initial and six month results". *Facial Plast Surg Clin North Am*, 2012. 20(2): p. 163-76.
- Calderhead et al., "One Mechanism Behind LED Photo-Therapy for Wound Healing and Skin Rejuvenation: Key Role of the Mast Cell" *Laser Therapy* 17.3: 141-148 (2008).
- Carruthers et al., "Consensus Recommendations for Combined Aesthetic Interventions in the Face Using Botulinum Toxin, Fillers, and Energy-Based Devices" *Dermatol Surg* 2016 (pp. 1-12).
- Casabona, G., et. al., "Microfocused Ultrasound with Visualization and Calcium Hydroxylapatite for Improving Skin Laxity and Cellulite Appearance"; *Plast Reconstr Surg Glob Open*. Jul. 25, 2017;5(7):e1388, 8 pages.
- Casabona, G., et. al., "Microfocused Ultrasound With Visualization and Fillers for Increased Neocollagenesis: Clinical and Histological Evaluation". *Dermatol Surg* 2014;40:S194-S198.
- Chan, N.P., et al., "Safety study of transcutaneous focused ultrasound for non-invasive skin tightening in Asians". *Lasers Surg Med*, 2011. 43(5): p. 366-75.
- Chapelon et al., "Effects of Cavitation in the High Intensity Therapeutic Ultrasound", *Ultrasonics Symposium*—1357 (1991).
- Chapelon, et al., "Thresholds for Tissue Ablation by Focused Ultrasound" (1990).
- Chen, L. et al., "Effect of Blood Perfusion on the ablation of liver parenchyma with high intensity focused ultrasound," *Phys. Med. Biol.* 38:1661-1673; 1993b.
- Coon, Joshua et al., "Protein identification using sequential ion/ion reactions and tandem mass spectrometry" *Proceedings of the National Academy of Sciences of the USA*, vol. 102, No. 27, Jul. 27, 2005, pp. 9463-9468.
- Corry, Peter M., et al., "Human Cancer Treatment with Ultrasound", *IEEE Transactions on Sonics and Ultrasonics*, vol. SU-31, No. 5, Sep. 1984, pp. 444, 456.
- Damianou et al., "Application of the Thermal Dose Concept for Predicting the Necrosed Tissue Volume During Ultrasound Surgery," 1993 IEEE Ultrasound Symposium, pp. 1199-1202.
- Daum et al., Design and Evaluation of a Feedback Based Phased Array System for Ultrasound Surgery, *IEEE Transactions on Ultrasonics, Ferroelectrics, and Frequency Control*, vol. 45, No. 2, Mar. 1998, pp. 431-438.
- Davis, Brian J., et al., "An Acoustic Phase Shift Technique for the Non-Invasive Measurement of Temperature Changes in Tissues", 1985 Ultrasonics Symposium, pp. 921-924.
- Dayan, S.H., et al., "Prospective, Multi-Center, Pivotal Trial Evaluating the Safety and Effectiveness of Micro-Focused Ultrasound with Visualization (MFU-V) for Improvement in Lines and Wrinkles of the Décolletage". *Plast Reconstr Surg*. Oct. 2014; 134(4 Suppl 1):123-4.
- Decision of the Korean Intellectual Property Tribunal dated Jun. 28, 2013 regarding Korean Patent No. 10-1142108, which is related to the pending application and/or an application identified in the Table on pp. 1-4 of the Information Disclosure Statement herein (English translation, English translation certification, and Korean decision included).
- Delon Martin, C., et al., "Venous Thrombosis Generation by Means of High-Intensity Focused Ultrasound" *Ultrasound in Med. & Biol.*, vol. 21, No. 1, pp. 113-119 (1995).
- Dierickx, Christine C., "The Role of Deep Heating for Noninvasive Skin Rejuvenation" *Lasers in Surgery and Medicine* 38:799-807 (2006).
- Dobke, M.K., et al., "Tissue restructuring by energy-based surgical tools". *Clin Plast Surg*, 2012. 39(4): p. 399-408.
- Dong, Yuan-Lin et al., "Effect of Ibuprofen on the Inflammatory Response to Surgical Wounds" *The Journal of Trauma*, vol. 35, No. 3. (1993).
- Dvivedi, Sanjay, et al. "Effect of Ibuprofen and diclofenac sodium on experimental wound healing" *Indian Journal of Experimental Biology*, vol. 35, pp. 1243-1245. (Nov. 1997).
- Fabi, S.G., "Microfocused Ultrasound With Visualization for Skin Tightening and Lifting: My Experience and a Review of the Literature". *Dermatol Surg*. Dec. 2014; 40 Suppl 12:S164-7.
- Fabi, S.G., "Noninvasive skin tightening: focus on new ultrasound techniques". *Clin Cosmet Investig Dermatol*. Feb. 5, 2015; 8:47-52.
- Fabi, S.G., et. al., "A prospective multicenter pilot study of the safety and efficacy of microfocused ultrasound with visualization for improving lines and wrinkles of the décolleté". *Dermatol Surg*. Mar. 2015; 41(3):327-35.
- Fabi, S.G., et. al., "Evaluation of microfocused ultrasound with visualization for lifting, tightening, and wrinkle reduction of the décolletage". *J Am Acad Dermatol*, 2013. 69(6): p. 965-71.
- Fabi, S.G., et. al., "Future directions in cutaneous laser surgery". *Dermatol Clin*, 2014. 32(1): p. 61-9.
- Fabi, S.G., et. al., "Retrospective Evaluation of Micro-focused Ultrasound for Lifting and Tightening the Face and Neck". *Dermatol Surg*, 2014.
- Friedmann D.P., "Comments on evaluation of microfocused ultrasound system for improving skin laxity and tightening in the lower face". *Aesthet Surg J*. Mar. 2015;35(3):NP81-2.
- Friedmann, D.P., et. al., "Combination of intense pulsed light, Sculptra, and Ultherapy for treatment of the aging face". *J Cosmet Dermatol*, 2014. 13(2): p. 109-18.
- Fry, W.J. et al., "Production of Focal Destructive Lesions in the Central Nervous System with Ultrasound," *J. Neurosurg.*, 11:471-478; 1954.
- Fujimoto, et al., "A New Cavitation Suppression Technique for Local Ablation Using High-Intensity Focused Ultrasound" *Ultrasonics Symposium*—1629 (1995).
- Gliklich et al., Clinical Pilot Study of Intense Ultrasound therapy to Deep Dermal Facial Skin and Subcutaneous Tissues, *Arch Facial Plastic Surgery*, Mar. 1, 2007, vol. 9, No. 1.
- Gold, M.H., et. al., "Use of Micro-Focused Ultrasound with Visualization to Lift and Tighten Lax Knee Skin". *J Cosmet Laser Ther*, 2014: p. 1-15.
- Goldberg, D.J., et. al., "Safety and Efficacy of Microfocused Ultrasound to Lift, Tighten, and Smooth the Buttocks". *Dermatol Surg* 2014; 40:1113-1117.
- Greene, R.M., et al., "Skin tightening technologies". *Facial Plast Surg*. Feb. 2014; 30(1):62-7.
- Greenhalgh, David G., "Wound healing and diabetes mellitus" *Clinics in Plastic Surgery* 30; 37-45. (2003).
- Guo, S. et al., "Factors Affecting Wound Healing" *Critical Reviews in Oral Biology & Medicine*, *J Dent Res* 89(3), pp. 219-229. (2010).
- Haar, G.R. et al., "Tissue Destruction with Focused Ultrasound in Vivo," *Eur. Urol.* 23 (suppl. 1):8-11; 1993.
- Hantash, Basil M. et al., "Bipolar Fractional Radiofrequency Treatment Induces Neocollagenesis and Neocollagenesis" *Lasers in Surgery and Medicine* 41:1-9 (2009).
- Hantash, Basil M. et al., "In Vivo Histological Evaluation of a Novel Ablative Fractional Resurfacing Device" *Lasers in Surgery and Medicine* 39:96-107 (2007).
- Harris, M.O., "Safety of Microfocused Ultrasound With Visualization in Patients With Fitzpatrick Skin Phototypes III to VI". *JAMA Facial Plast. Surg*, 2015.
- Hart, et. al., "Current Concepts in the Use of PLLA: Clinical Synergy Noted with Combined Use of Microfocused Ultrasound and Poly-L-Lactic Acid on the Face, Neck, and Décolletage". *Amer. Soc. Plast. Surg*. 2015. 136; 180-187S.
- Hassan et al., "Structure and Applications of Poly(vinyl alcohol) Hydrogels Produced by Conventional Crosslinking or by Freezing/Thawing Methods," *advanced in Polymer Science*, 2000, pp. 37-65, vol. 153.
- Hassan et al., "Structure and Morphology of Freeze/Thawed PVA Hydrogels," *Macromolecules*, Mar. 11, 2000, pp. 2472-2479, vol. 33, No. 7.
- Hessel et al., "A Validated Photonic Cellulite Severity Scale"; *J Eur Acad Dermatol Venereol*. May 2009; 23(5):523-8, 6 pages.
- Hitchcock, T.M. et. al., "Review of the safety profile for microfocused ultrasound with visualization". *Journal of Cosmetic Dermatology*, 13, 329-335. (2014).

(56)

References Cited

OTHER PUBLICATIONS

- Husseini et al., "The Role of Cavitation in Acoustically Activated Drug Delivery," *J. Control Release*, Oct. 3, 2005, pp. 253-261, vol. 107(2).
- Husseini et al., "Investigating the mechanism of acoustically activated uptake of drugs from Pluronic micelles," *BMD Cancer* 2002, 2:20k, Aug. 30, 2002, pp. 1-6.
- Hynynen et al., "Temperature Distributions During Local Ultrasound Induced Hyperthermia In Vivo," *Ultrasonics Symposium—745* (1982).
- Jeffers et al., "Evaluation of the Effect of Cavitation Activity on Drug-Ultrasound Synergisms," 1993 IEEE Ultrasonics Symposium, pp. 925-928.
- Jenne, J., et al., "Temperature Mapping for High Energy US-Therapy," 1994 Ultrasonics Symposium, pp. 1879-1882.
- Jeong, K.H., et al., "Neurologic complication associated with intense focused ultrasound". *J Cosmet Laser Ther*, 2013.
- Johnson, S.A., et al., "Non-Intrusive Measurement of Microwave and Ultrasound-Induced Hyperthermia by Acoustic Temperature Tomography", *Ultrasonics Symposium Proceedings*, pp. 977-982. (1977).
- Kim, H.J., et al., "Coagulation and ablation patterns of high-intensity focused ultrasound on a tissue mimicking phantom and cadaveric skin". *Laser Med Sci*. Sep. 4, 2015.
- Kornstein, A.N., "Ulthera for silicone lip correction". *Plast Reconstr Surg*, 2012. 129(6): p. 1014e-1015e.
- Kornstein, A.N., "Ultherapy shrinks nasal skin after rhinoplasty following failure of conservative measures". *Plast Reconstr Surg*, 2013. 131(4): p. 664e-6e.
- Krischak, G.D., et al., "The effects of non-steroidal anti-inflammatory drug application on incisional wound healing in rats" *Journal of Wound Care*, vol. 6, No. 2, (Feb. 2007).
- Laubach, H.J., et al., "Confined Thermal Damage with Intense Ultrasound (IUS)" [abstr.] *American Society for Laser Medicine and Surgery Abstracts*, p. 15 #43 (Apr. 2006).
- Laubach, H.J., et al., "Intense focused ultrasound: evaluation of a new treatment modality for precise microcoagulation within the skin". *Dermatol Surg*, 2008. 34(5): p. 727-34.
- Lee, H.J., et al., "The efficacy and safety of intense focused ultrasound in the treatment of enlarged facial pores in Asian skin". *J Dermatolog Treat*, 2014.
- Lee, H.S., et al., "Multiple Pass Ultrasound Tightening of Skin Laxity of the Lower Face and Neck". *Dermatol Surg*, 2011.
- Lin, Sung-Jan, et al., "Monitoring the thermally induced structural transitions of collagen by use of second-harmonic generation microscopy" *Optics Letters*, vol. 30, No. 6, (Mar. 15, 2005).
- Macgregor J.L., et al., "Microfocused Ultrasound for Skin Tightening". *Semin Cutan Med Surg* 32:18-25. (2013).
- Madersbacher, S. et al., "Tissue Ablation in Benign Prostatic Hyperplasia with High Intensity Focused Ultrasound," *Dur. Urol.*, 23 (suppl. 1):39-43; 1993.
- Makin et al., "B-Scan Imaging and Thermal Lesion Monitoring Using Miniaturized Dual-Functionality Ultrasound Arrays," *Ultrasonics Symposium*, 2004 IEEE, Aug. 23, 2004, pp. 1788-1791, vol. 3.
- Makin et al., "Confirmed Bulk Ablation and Therapy Monitoring Using Intracorporeal Image-Treat Ultrasound Arrays," 4th International Symposium on Therapeutic Ultrasound, Sep. 19, 2004.
- Makin et al., "Miniaturized Ultrasound Arrays for Interstitial Ablation and Imaging," *UltraSound Med. Biol.* 2005, Nov. 1, 2005, pp. 1539-1550, vol. 31(11).
- Manohar et al., "Photoacoustic mammography laboratory prototype: imaging of breast tissue phantoms," *Journal of Biomedical Optics*, Nov./Dec. 2004, pp. 1172-1181, vol. 9, No. 6.
- Mast et al., "Bulk Ablation of Soft Tissue with Intense Ultrasound; Modeling and Experiments," *J. Acoust. Soc. Am.*, Oct. 1, 2005, pp. 2715-2724, vol. 118(4).
- Meshkinpour, Azin, et al., "Treatment of Hypertrophic Scars and Keloids With a Radiofrequency Device: A Study of Collagen Effects" *Lasers in Surgery and Medicine* 37:343-349 (2005).
- Minkis, K., et. al., "Ultrasound skin tightening". *Dermatol Clin*, 2014. 32(1): p. 71-7.
- Mitragotri, S., "Healing sound: the use of ultrasound in drug delivery and other therapeutic applications," *Nature Reviews; Drug Delivery*, pp. 255-260, vol. 4 (Mar. 2005).
- Mosser, David M. et al., "Exploring the full spectrum of macrophage activation" *Nat Rev Immunol*; 8(12): 958-969. (Dec. 2008).
- Murota, Sei-Itsu, et al., "Stimulatory Effect of Prostaglandins on the Production of Hexosamine-Containing Substances by Cultured Fibroblasts (3) Induction of Hyaluronic Acid Synthetase by Prostaglandin" Department of Pharmacology, Tokyo Metropolitan Institute of Gerontology, Itabashiku, Tokyo-173, Japan. (Nov. 1977, vol. 14, No. 5).
- Murota, Sei-Itsu, et al., "The Stimulatory Effect of Prostaglandins on Production of Hexosamine-Containing Substances by Cultured Fibroblasts" Department of Pharmacology, Tokyo Metropolitan Institute of Gerontology, Itabashiku, Tokyo-173, Japan. (Aug. 1976, vol. 12, No. 2).
- Nestor, M.S. et al., "Safety and Efficacy of Micro-focused Ultrasound Plus Visualization for the Treatment of Axillary Hyperhidrosis". *J Clin Aesthet Dermatol*, 2014. 7(4): p. 14-21.
- Oni, G., et. al. "Response to 'comments on evaluation of microfocused ultrasound system for improving skin laxity and tightening in the lower face'". *Aesthet Surg J*. Mar. 2015;35(3):NP83-4.
- Oni, G., et. al., "Evaluation of a Microfocused Ultrasound System for Improving Skin Laxity and Tightening in the Lower Face". *Aesthet Surg J*, 2014. 38:861-868.
- Pak, C.S., et. al., "Safety and Efficacy of Ulthera in the Rejuvenation of Aging Lower Eyelids: A Pivotal Clinical Trial". *Aesthetic Plast Surg*, 2014.
- Paradossi et al., "Poly(vinyl alcohol) as versatile biomaterial for potential biomedical applications," *Journal of Materials Science: Materials in Medicine*, 2003, pp. 687-691, vol. 14.
- Pritzker, R.N., et. al., "Updates in noninvasive and minimally invasive skin tightening", *Semin Cutan Med Surg*. Dec. 2014;33(4):182-7.
- Pritzker, R.N., et. al., "Comparison of different technologies for noninvasive skin tightening". *Journal of Cosmetic Dermatology*, 13, 315-323. (2014).
- Rappolee, Daniel A., et al., "Wound Macrophages Express TGF and Other Growth Factors in Vivo: Analysis by mRNA Phenotyping" *Science*, vol. 241, No. 4866 (Aug. 1988).
- Reid, Gavin, et al., "Tandem Mass spectrometry of ribonuclease A and B: N-linked glycosylation site analysis of whole protein ions," *Analytical Chemistry*. Feb. 1, 2002, vol. 74, No. 3, pp. 577-583.
- Righetti et al., "Elastographic Characterization of HIFU-Induced Lesions in Canine Livers," 1999, *Ultrasound in Med & Bio*, vol. 25, No. 7, pp. 1099-1113.
- Rokhsar, C., et. al., "Safety and efficacy of microfocused ultrasound in tightening of lax elbow skin". *Dermatol Surg*. 2015; 41(7):821-6.
- Rosenberg, Carol S. "Wound Healing in the Patient with Diabetes Mellitus" *Nursing Clinics of North America*, vol. 25, No. 1, (Mar. 1990).
- Saad et al., "Ultrasound-Enhanced Effects of Adriamycin Against Murine Tumors," *Ultrasound in Med. & Biol.* vol. 18, No. 8, pp. 715-723 (1992).
- Sabet-Peyman, E.J. et. al., "Complications Using Intense Ultrasound Therapy to Treat Deep Dermal Facial Skin and Subcutaneous Tissues". *Dermatol Surg* 2014; 40:1108-1112.
- Sandulache, Vlad C. et al., "Prostaglandin E2 inhibition of keloid fibroblast migration, contraction, and transforming growth factor (TGF)- β 1-induced collagen synthesis" *Wound Rep Reg* 15 122-133, 2007. (2007).
- Sanghvi, N.T., et al., "Transrectal Ablation of Prostate Tissue Using Focused Ultrasound," 1993 *Ultrasonics Symposium*, IEEE, pp. 1207-1210.
- Sasaki, G.H. et. al., "Clinical Efficacy and Safety of Focused-Image Ultrasonography: A 2-Year Experience". *Aesthet Surg J*, 2012.
- Sasaki, G.H. et. al., "Microfocused Ultrasound for Nonablative Skin and Subdermal Tightening to the Periorbital and Body Sites: Preliminary Report on Eighty-Two Patients". *Journal of Cosmetics, Dermatological Sciences and Applications*, 2012, 2, 108-116.

(56)

References Cited

OTHER PUBLICATIONS

- Sassen, Sander, "ATI's R520 architecture, the new king of the hill?" <http://www.hardwareanalysis.com/content/article/1813>, Sep. 16, 2005, 2 pages.
- Seip, Ralf, et al., "Noninvasive Detection of Thermal Effects Due to Highly Focused Ultrasonic Fields," IEEE Symposium, pp. 1229-1232, vol. 2, Oct. 3-Nov. 1993.
- Seip, Ralf, et al., "Noninvasive Estimation of Tissue Temperature Response to Heating Fields Using Diagnostic Ultrasound," IEEE Transactions on Biomedical Engineering, vol. 42, No. 8, Aug. 1995, pp. 828-839.
- Simon et al., "Applications of Lipid-Coated Microbubble Ultrasonic Contrast to Tumor Therapy," Ultrasound in Med. & Biol. vol. 19, No. 2, pp. 123-125 (1993).
- Sklar, L.R., et al., "Use of transcutaneous ultrasound for lipolysis and skin tightening: a review". Aesthetic Plast Surg, 2014. 38(2): p. 429-41.
- Smith, Nadine Barrie, et al., "Non-invasive In Vivo Temperature Mapping of Ultrasound Heating Using Magnetic Resonance Techniques", 1994 Ultrasonics Symposium, pp. 1829-1832, vol. 3.
- Suh, D.H. et al., "A intense-focused ultrasound tightening for the treatment of infraorbital laxity". J Cosmet Laser Ther, 2012. 14(6): p. 290-5.
- Suh, D.H., et al., "Comparative histometric analysis of the effects of high-intensity focused ultrasound and radiofrequency on skin". J Cosmet Laser Ther. Mar. 24, 2015:1-7.
- Suh, D.H., et al., "Intense Focused Ultrasound Tightening in Asian Skin: Clinical and Pathologic Results" American Society for Dermatologic Surgery, Inc.; 37:1595-1602. (2011).
- Surry et al., "Poly(vinyl alcohol) cryogel phantoms for use in ultrasound and MR imaging," Phys. Med. Biol., Dec. 6, 2004, pp. 5529-5546, vol. 49.
- Syka J. E. P. et al., "Peptide and Protein Sequence Analysis by Electron Transfer Dissociation Mass Spectrometry," Proceedings of the National Academy of Sciences of USA, National Academy of Science, Washington, DC, vol. 101, No. 26, Jun. 29, 2004, pp. 9528-9533.
- Talbert, D. G., "An Add-On Modification for Linear Array Real-Time Ultrasound Scanners to Produce 3D Displays," UTS Int'l 1977 Brighton, England (Jun. 28-30, 1977) pp. 57-67.
- Tata et al., "Interaction of Ultrasound and Model Membrane Systems: Analyses and Predictions," American Chemical Society, Phys. Chem. 1992, 96, pp. 3548-3555.
- Ueno, S., et al., "Ultrasound Thermometry in Hyperthermia", 1990 Ultrasonic Symposium, pp. 1645-1652.
- Verhofstad, Michiel H.J. et al., "Collagen Synthesis in rat skin and ileum fibroblasts is affected differently by diabetes-related factors" Int. J. Exp. Path. (1998), 79, 321-328.
- Wang, H., et al., "Limits on Focused Ultrasound for Deep Hyperthermia", 1994 Ultrasonic Symposium, Nov. 1-4, 1994, pp. 1869-1872, vol. 3.
- Wasson, Scott, "NVIDIA's GeForce 7800 GTX graphics processor Power MADD," <http://techreport.com/reviews/2005q2/geforce-7800gtx/index.x?pg=1>, Jun. 22, 2005, 4 pages.
- Weiss, M., "Commentary: noninvasive skin tightening: ultrasound and other technologies: where are we in 2011?" Dermatol Surg, 2012. 38(1): p. 28-30.
- White et al "Selective Creating of Thermal Injury Zones in the Superficial Musculoaponeurotic System Using Intense Ultrasound Therapy," Arch Facial Plastic Surgery, Jan./Feb. 2007, vol. 9, No. 1 (pp. 22-29).
- White, W. M., et al., "Selective Transcutaneous Delivery of Energy to Facial Subdermal Tissues Using the Ultrasound Therapy System" [abstr]. American Society for Laser Medicine and Surgery Abstracts, p. 37 #113 (Apr. 2006).
- White, W. Matthew, et al., "Selective Transcutaneous Delivery of Energy to Porcine Soft Tissues Using Intense Ultrasound (IUS)" Lasers in Surgery and Medicine 40:67-75 (2008).
- Woodward, J.A., et al. "Safety and Efficacy of Combining Microfocused Ultrasound With Fractional CO2 Laser Resurfacing for Lifting and Tightening the Face and Neck". Dermatol Surg, Dec. 2014 40:S190-S193.
- Zelickson, Brian D. et al., "Histological and Ultrastructural Evaluation of the Effects of a Radiofrequency-Based Nonablative Dermal Remodeling Device, A Pilot Study" Arch Dermatol, vol. 140, (Feb. 2004).
- Ulthera, Inc., Petition for Inter Partes Review filed Jul. 19, 2016 in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 63 pages (Filed Jul. 19, 2016).
- Ulthera Exhibit 1001, U.S. Pat. No. 6,113,559 to Klopotek, filed Jul. 19, 2016 in re IPR2016-01459.
- Ulthera Exhibit 1002, Patent file history of U.S. Pat. No. 6,113,559 Klopotek filed Jul. 19, 2016 in re IPR2016-01459.
- Ulthera Exhibit 1003, Declaration of Expert Witness Mark E. Schafer, Ph.D. filed Jul. 19, 2016 in re IPR2016-01459.
- Ulthera Exhibit 1004, Curriculum Vitae of Mark E. Schafer, Ph.D. filed Jul. 19, 2016 in re IPR2016-01459.
- Ulthera Exhibit 1005, International PCT Publication WO96/34568 Knowlton filed Jul. 19, 2016 in re IPR2016-01459.
- Ulthera Exhibit 1006, French Patent No. 2,672,486, Technomed patent filed Jul. 19, 2016 in re IPR2016-01459.
- Ulthera Exhibit 1007, English translation of French Patent No. 2,672,486, Technomed filed Jul. 19, 2016 in re IPR2016-01459.
- Ulthera Exhibit 1008, International PCT Publication WO93/12742, Technomed PCT filed Jul. 19, 2016 in re IPR2016-01459.
- Ulthera Exhibit 1009, English translation of International PCT Publication WO93/12742, Technomed PCT filed Jul. 19, 2016 in re IPR2016-01459.
- Ulthera Exhibit 1010, U.S. Pat. No. 5,601,526, which claims priority to Technomed PCT filed Jul. 19, 2016 in re IPR2016-01459.
- Ulthera Exhibit 1011, Patent file history for European Patent Application No. 98964890.2, Klopotek filed Jul. 19, 2016 in re IPR2016-01459.
- Ulthera Exhibit 1012, Translator Declaration filed Jul. 19, 2016 in re IPR2016-01459.
- Ulthera Exhibit 1013, U.S. Pat. No. 5,230,334 to Klopotek filed Jul. 19, 2016 in re IPR2016-01459.
- Ulthera Exhibit 1014, U.S. Pat. No. 5,755,753 to Knowlton filed Jul. 19, 2016 in re IPR2016-01459.
- Ulthera Exhibit 1015, Excerpts from the American Medical Association Encyclopedia of Medicine (1989) filed Jul. 19, 2016 in re IPR2016-01459.
- Ulthera Exhibit 1016, The Simultaneous Study of Light Emissions and Shock Waves Produced by Cavitation Bubbles, G. Gimenez, J. Acoust. Soc. Am. 71(4), Apr. 1982, pp. 839-847 (filed Jul. 19, 2016 in re IPR2016-01459).
- Ulthera Exhibit 1017, Excerpts from Gray's Anatomy (1995) (filed Jul. 19, 2016 in re IPR2016-01459).
- Ulthera Exhibit 1018, Anatomy of the Superficial Venous System, Comjen G.M., Dermatol. Surg., 1995; 21:35-45 (filed Jul. 19, 2016 in re IPR2016-01459).
- Ulthera Exhibit 1019, Section 2.6 from Ultrasonics Theory and Application, by G.L. Gooberman (Hart Publishing Co., 1969) (filed Jul. 19, 2016 in re IPR2016-01459).
- Ulthera Exhibit 1020, Deep Local Hyperthermia for Cancer Therapy: External Electromagnetic and Ultrasound Techniques, A.Y. Cheung and A. Neyzari, Cancer Research (Suppl.), vol. 44, pp. 4736-4744 (1984) (filed Jul. 19, 2016 in re IPR2016-01459).
- Decision on Institution of Inter Partes Review in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 20 pages [011] (Dated Jan. 23, 2017).
- Dermafocus Response to Institution of Inter Partes Review in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 73 pages [018] (Dated Apr. 26, 2017).
- Dermafocus Exhibit List in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 5 pages [019] (Dated Apr. 26, 2017).
- Dermafocus Exhibit 2002, Declaration of Mark Palmeri, in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 136 pages (Filed Apr. 26, 2017).
- Dermafocus Exhibit 2003, Deposition of Dr. Mark Schafer, in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 327 pages (Filed Apr. 26, 2017).

(56)

References Cited**OTHER PUBLICATIONS**

Dermafocus Exhibit 2004, Amendment No. 4 to Ulthera Form S-1, in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 308 pages (Filed Apr. 26, 2017).

Dermafocus Exhibit 2005, Excerpt from Churchill Livingstone, Gray's Anatomy (38th ed. 1995), in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 7 pages (Filed Apr. 26, 2017).

Dermafocus Exhibit 2006, Bo Eklof et al., "Revision of the CEAP Classification for Chronic Venous Disorders: Consensus Statement," ACTA FAC MED NAISS, vol. 25, No. 1 (2008), 3-10 in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 7 pages (Filed Apr. 26, 2017).

Dermafocus Exhibit 2007, WebMD, "Varicose Veins and Spider Veins" downloaded from <http://www.webmd.com/skin-problems-and-treatments/guide/varicose-spider-veins#1> in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 3 pages (Filed Apr. 26, 2017).

Dermafocus Exhibit 2008, John M. Porter et al., "Reporting Standards in Venous Disease: An Update," Journal of Vascular Surgery, vol. 21, No. 4 (1995), 635-645 in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 11 pages (Filed Apr. 26, 2017).

Dermafocus Exhibit 2009, Kullervo Hynynen, "Review of Ultrasound Therapy," 1997 Ultrasonics Symposium (1997), 1305-1313, in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 9 pages (Filed Apr. 26, 2017).

Dermafocus Exhibit 2010, A.G. Visioli et al., "Preliminary Results of a Phase I Dose Escalation Clinical Trial Using Focused Ultrasound in the Treatment of Localised Tumours," European Journal of Ultrasound, vol. 9 (1999), 11-18, in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 8 pages (Filed Apr. 26, 2017).

Dermafocus Exhibit 2011, U.S. Pat. No. 5,143,063, issued on Sep. 1, 1992, Fellner, in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 6 pages (Filed Apr. 26, 2017).

Dermafocus Exhibit 2012, Hugh G. Beebe et al., "Consensus Statement: Classification and Grading of Chronic Venous Disease in the Lower Limbs," European Journal of Vascular and Endovascular Surgery, vol. 12 (1996), 487-492, in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 6 pages (Filed Apr. 26, 2017).

Dermafocus Exhibit 2013, Excerpt from Mosby's Medical Dictionary (3rd ed. 1990), in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 4 pages (Filed Apr. 26, 2017).

Dermafocus Exhibit 2014, Excerpt from Miller-Keane Encyclopedia & Dictionary of Medicine, Nursing, & Allied Health (5th ed. 1992), in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 6 pages (Filed Apr. 26, 2017).

Dermafocus Exhibit 2015, David J. Tibbs et al., Varicose Veins, Venous Disorders, and Lymphatic Problems in the Lower Limbs (1997), Chapter 4: Clinical Patterns of Venous Disorder I, 47-67, in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 24 pages (Filed Apr. 26, 2017).

Dermafocus Exhibit 2016, Mitchel P. Goldman et al., Varicose Veins and Telangiectasias (2nd ed. 1999), Chapter 22: Treatment of Leg Telangiectasias with Laser and High-Intensity Pulsed Light, 470-497, in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 31 pages (Filed Apr. 26, 2017).

Dermafocus Exhibit 2017, Email from Anderson to Klopotek dated May 25, 2004, in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 1 page (Filed Apr. 26, 2017).

Dermafocus Exhibit 2018, List of Klopotek Patents, in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 411 pages (Filed Apr. 26, 2017).

Dermafocus Exhibit 2019, Declaration of Peter Klopotek Civil Action 15-cv-654-SLR, dated Nov. 2, 2016, in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 1 page (Filed Apr. 26, 2017).

Dermafocus Exhibit 2020, "Our Technology," downloaded from <http://jobs.ulthera.com/about> on Apr. 10, 2017, in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 4 pages (Filed Apr. 26, 2017).

Dermafocus Exhibit 2021, C. Damianou and K. Hynynen, "Focal Spacing and Near-Field Heating During Pulsed High Temperature Ultrasound Therapy," Ultrasound in Medicine & Biology, vol. 19, No. 9 (1993), 777-787, in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 11 pages (Filed Apr. 26, 2017).

Dermafocus Exhibit 2022, Excerpt from Mosby's Medical Dictionary (5th ed. 1997), in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 5 pages (Filed Apr. 26, 2017).

Dermafocus Exhibit 2023, Excerpt from Miller-Keane Encyclopedia & Dictionary of Medicine, Nursing, & Allied Health (6th ed. 1997), in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 7 pages (Filed Apr. 26, 2017).

Dermafocus Exhibit 2024, Excerpt from Stedman's Concise Medical Dictionary (3rd ed. 1997), in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 4 pages (Filed Apr. 26, 2017).

Dermafocus Exhibit 2025, Excerpt from Taber's Cyclopedic Medical Dictionary (18th ed. 1997), in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 9 pages (Filed Apr. 26, 2017).

Dermafocus Exhibit 2026, Bo Eklof et al., "Revision of the CEAP Classification for Chronic Venous Disorders: Consensus Statement," Journal of Vascular Surgery, vol. 40, No. 6 (2004), 1248-1252.e1, in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 6 pages (Filed Apr. 26, 2017).

Ulthera, Inc., Reply in Support of Petition for Inter Partes Review in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 33 pages (Filed Aug. 2, 2017).

Ulthera Exhibit 1022, Use of the Argon and Carbon Dioxide Lasers for Treatment of Superficial Venous Varicosities of the Lower Extremity, D. Apfelberg et al., Lasers in Surgery and Medicine, vol. 4.3, pp. 221-231 (1984) (filed Aug. 2, 2017 in re IPR2016-01459).

Ulthera Exhibit 1023, 532-Nanometer Green Laser Beam Treatment of Superficial Varicosities of the Lower Extremities, T. Smith et al., Lasers in Surgery and Medicine, vol. 8.2, pp. 130-134 (1988) (filed Aug. 2, 2017 in re IPR2016-01459).

Ulthera Exhibit 1024, Deposition Transcript of Dr. Mark Palmeri on Jul. 11, 2017 (filed Aug. 2, 2017 in re IPR2016-01459).

Ulthera Exhibit 1025, Ulthera Oral Proceeding Demonstrative Slides (filed Oct. 2, 2017 in re IPR2016-01459).

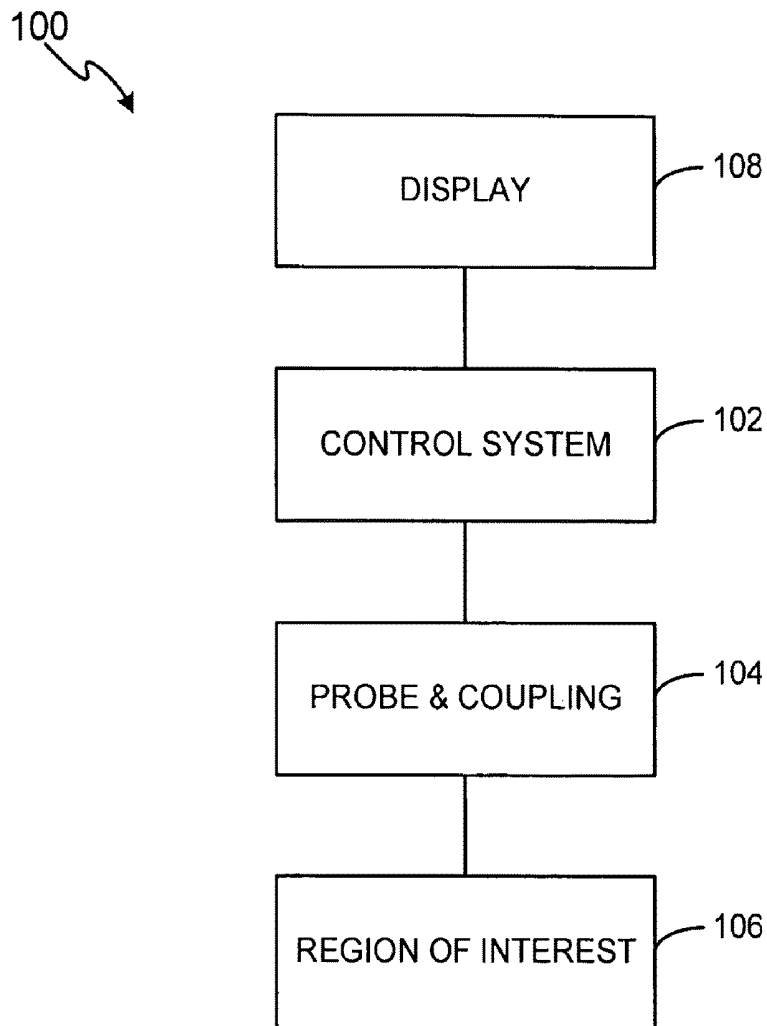
Dermafocus Exhibit 2027, DermaFocus Oral Proceeding Demonstrative Slides (filed Oct. 2, 2017 in re IPR2016-01459).

PTAB Record of Oral Hearing held Oct. 4, 2017 in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 67 pages (PTAB Document sent to Ulthera on Nov. 1, 2017).

Final Written Decision of Inter Partes Review in Re U.S. Pat. No. 6,113,559; IPR2016-01459; 37 pages [030] (Entered Jan. 19, 2018).

Microchip microID 125 kHz EFID System Design Guide, Microchip Technology Inc. (2004).

* cited by examiner

**FIG. 1**

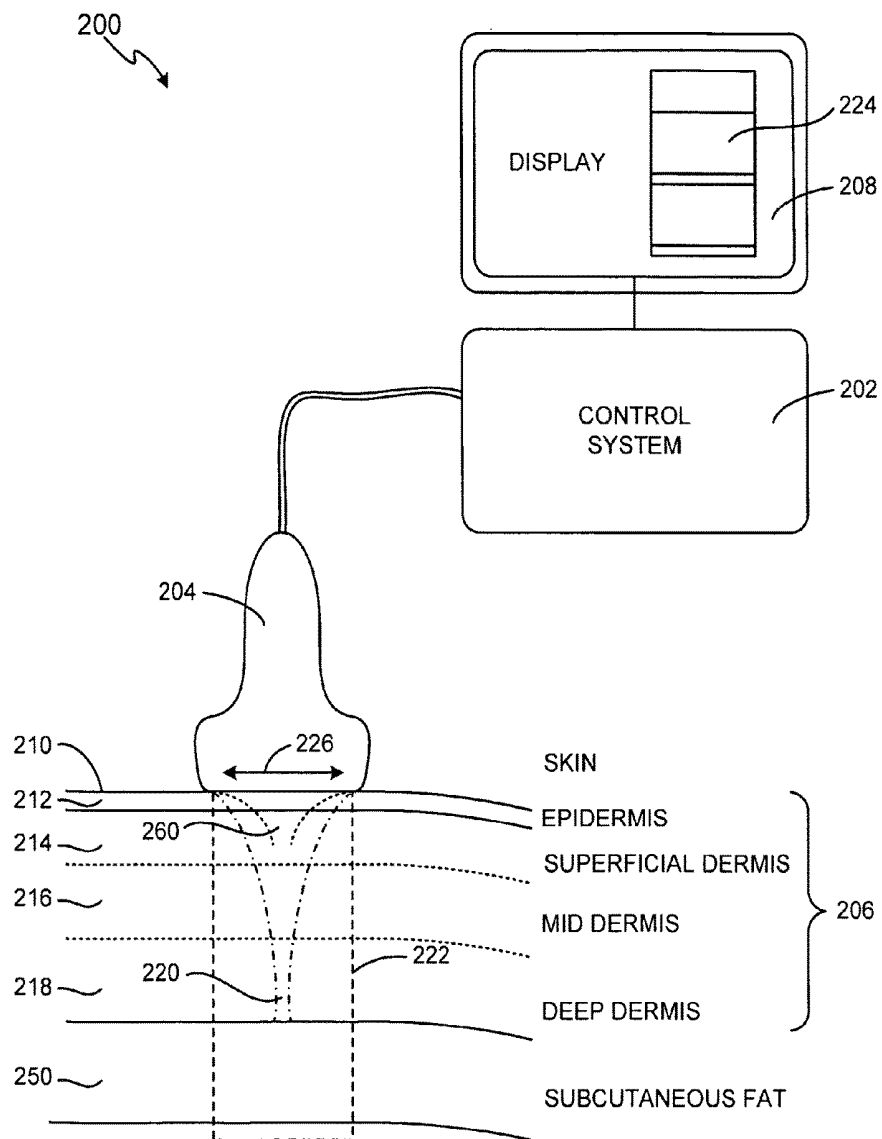


FIG. 2A

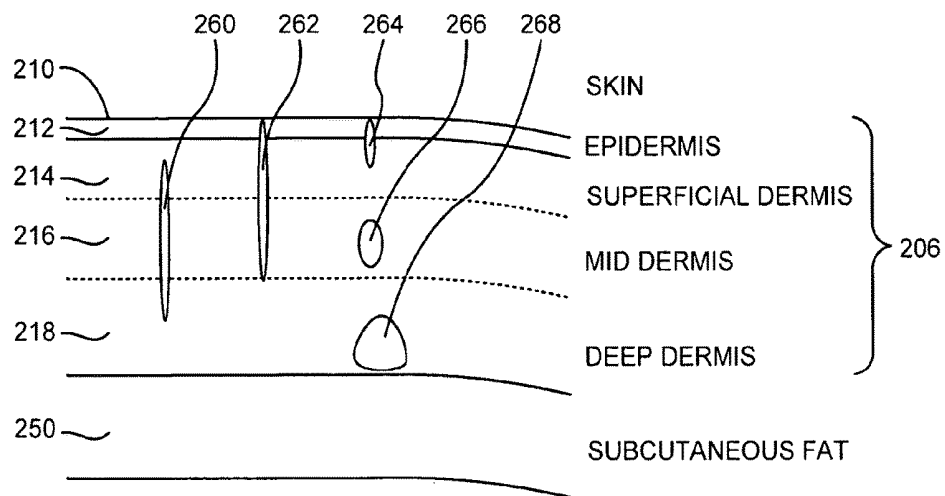


FIG. 2B

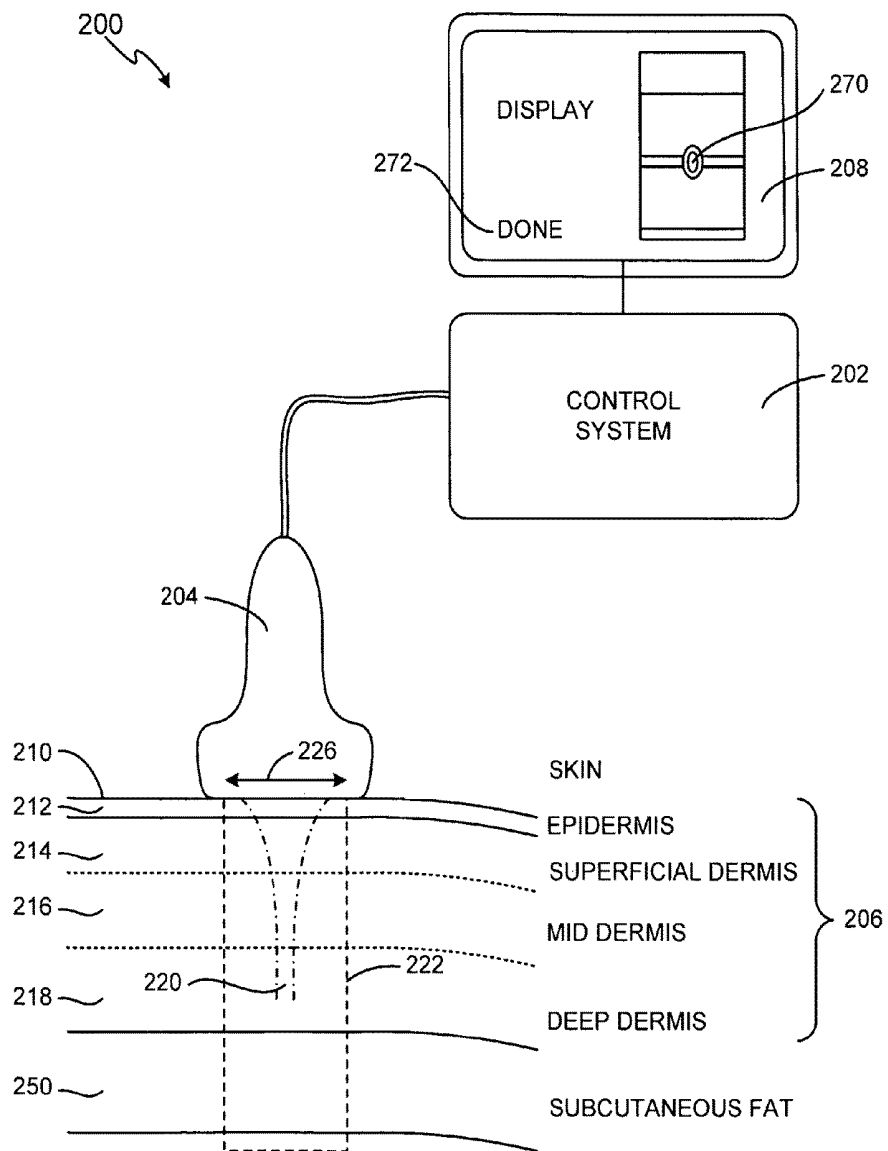


FIG. 2C

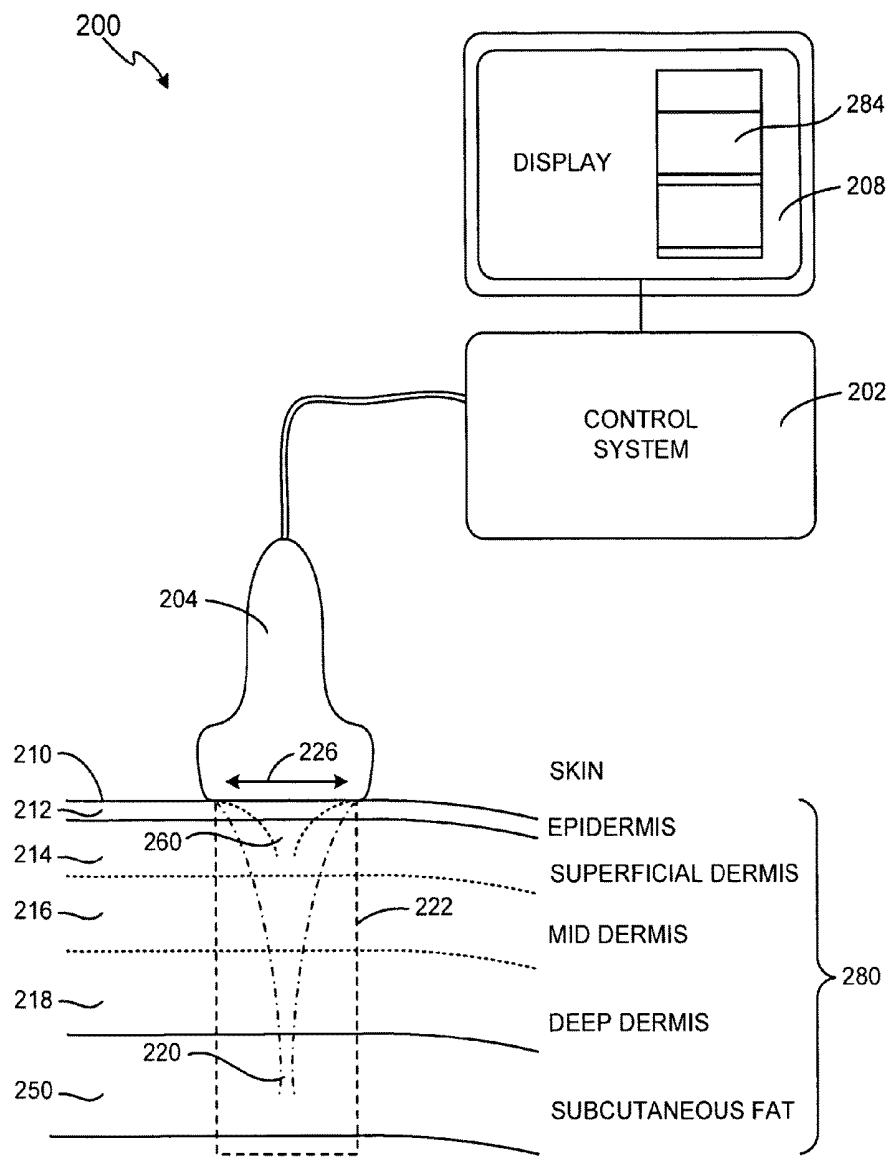
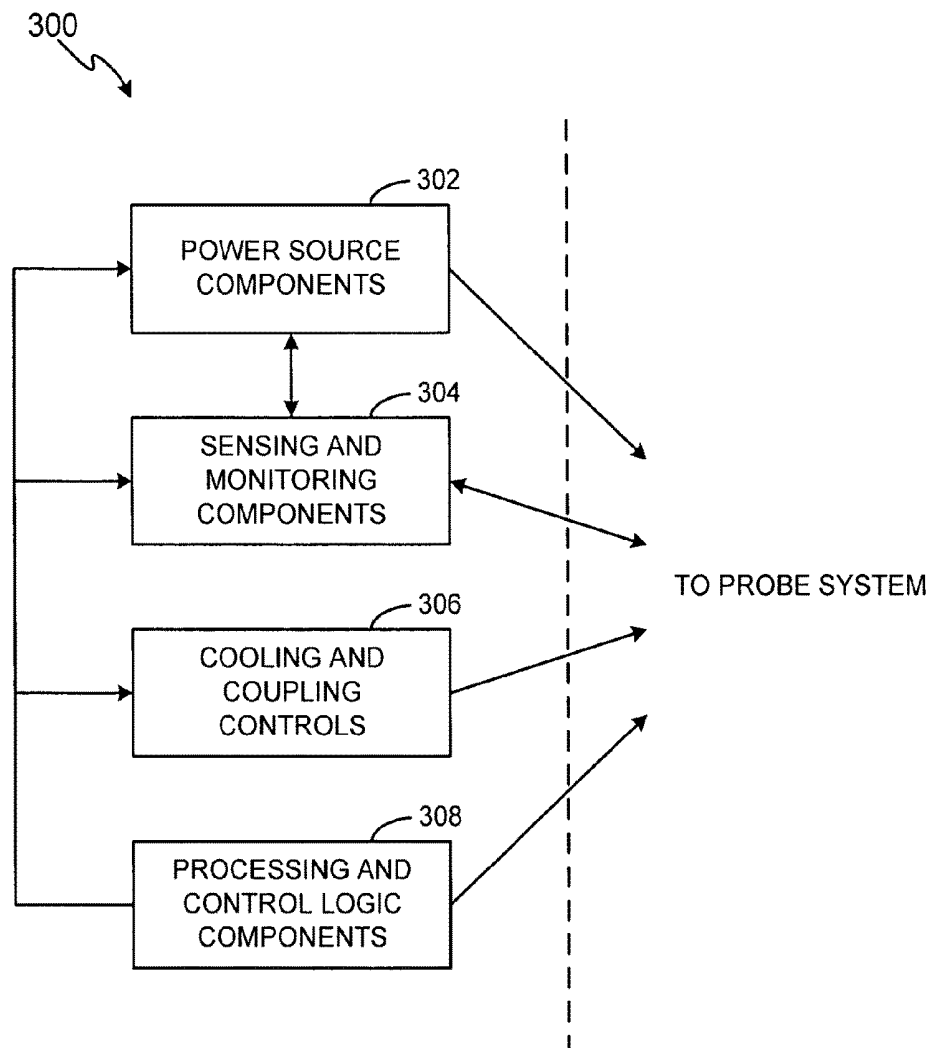
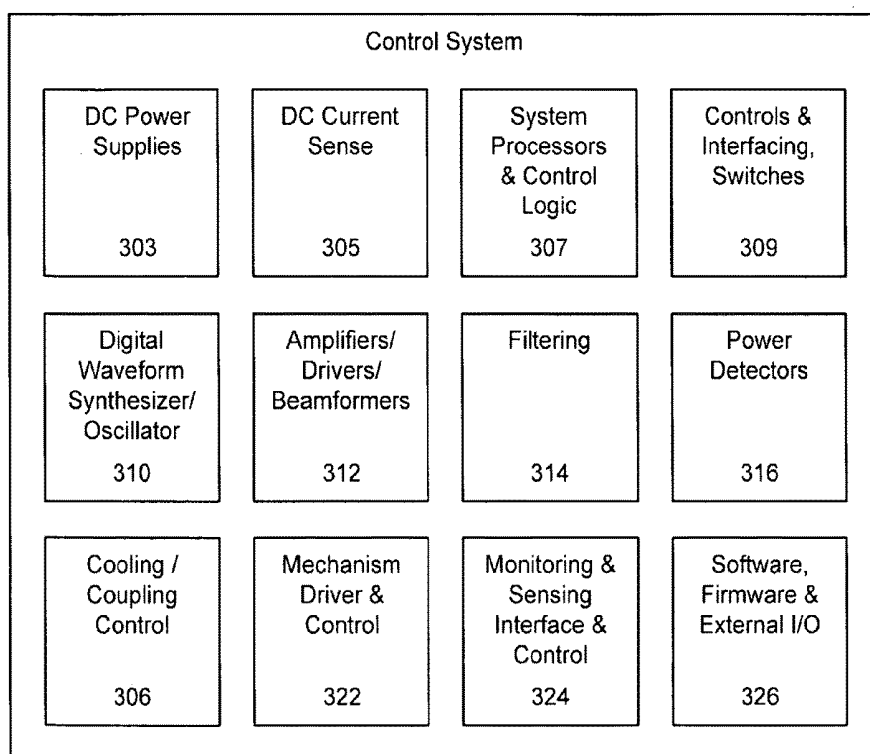
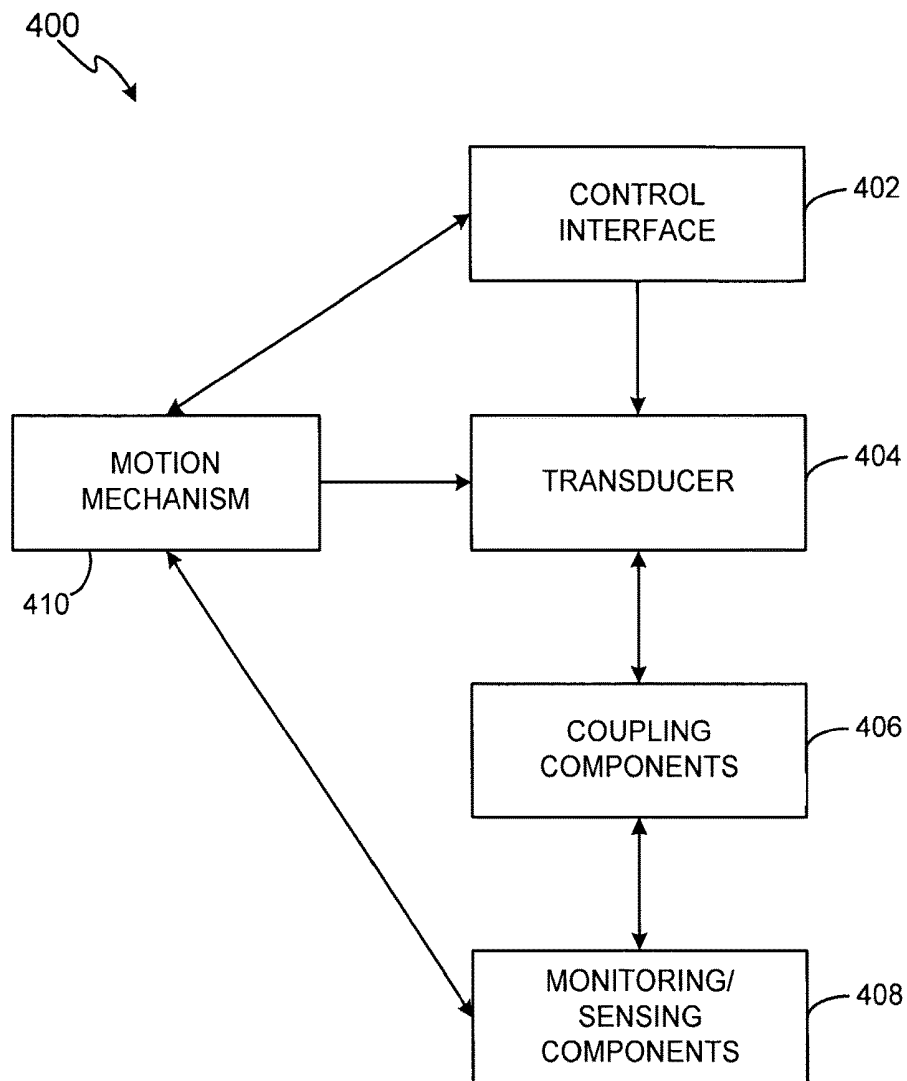


FIG. 2D

**FIG. 3A**

300
**FIG. 3B**

**FIG. 4A**

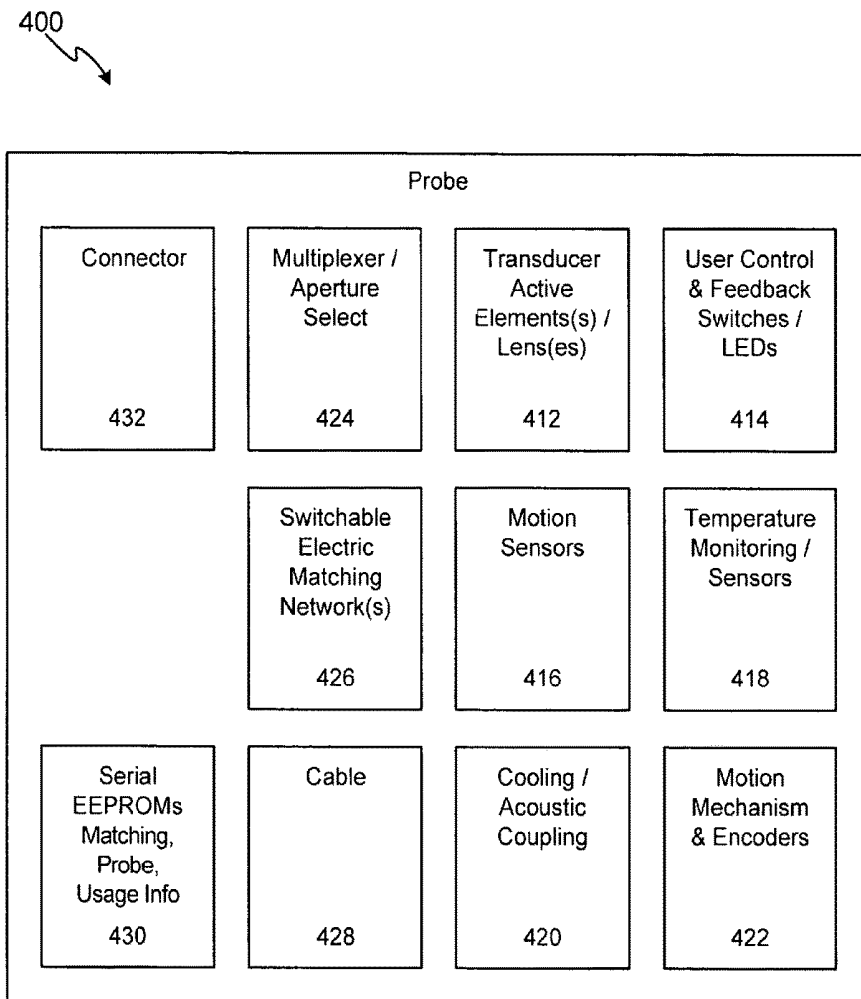


FIG. 4B

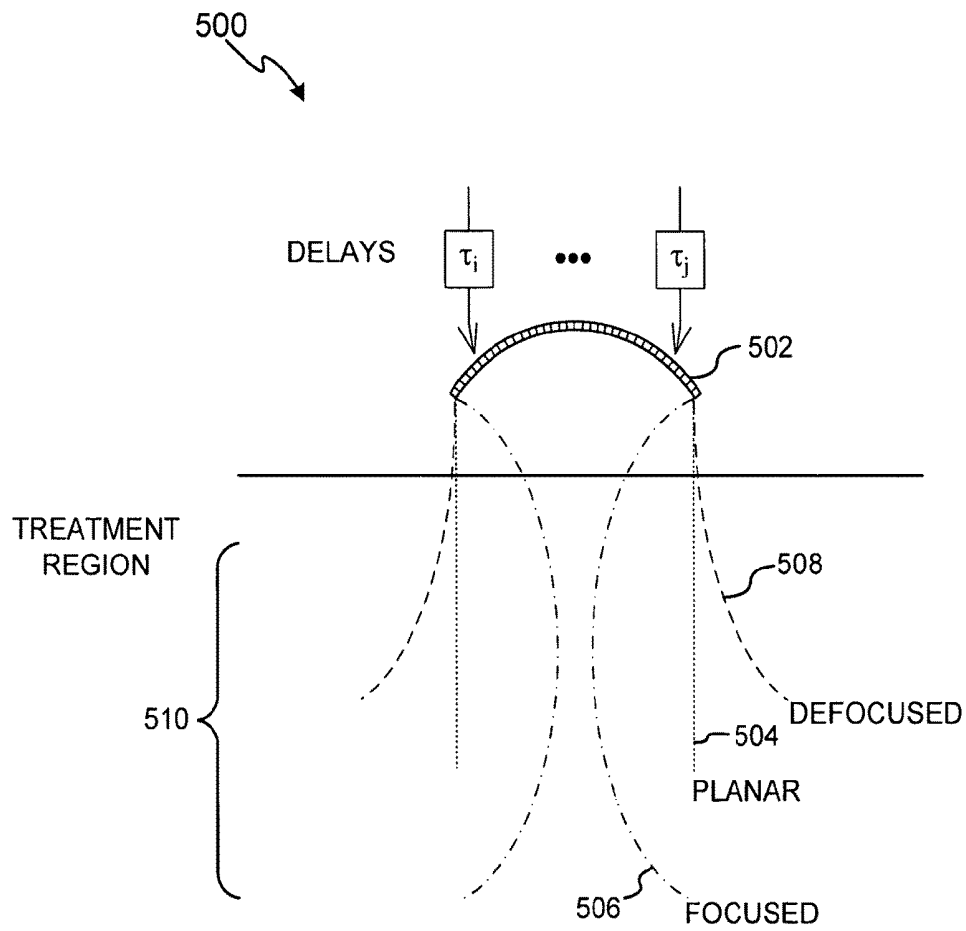
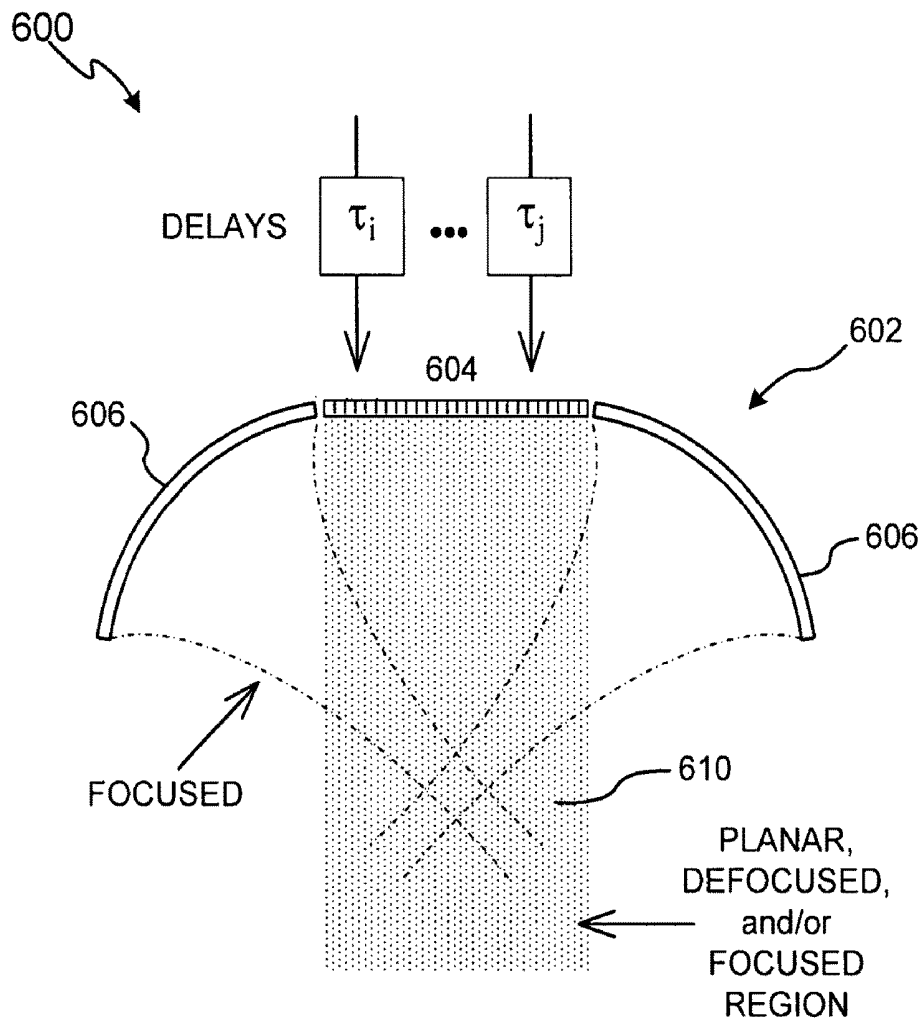
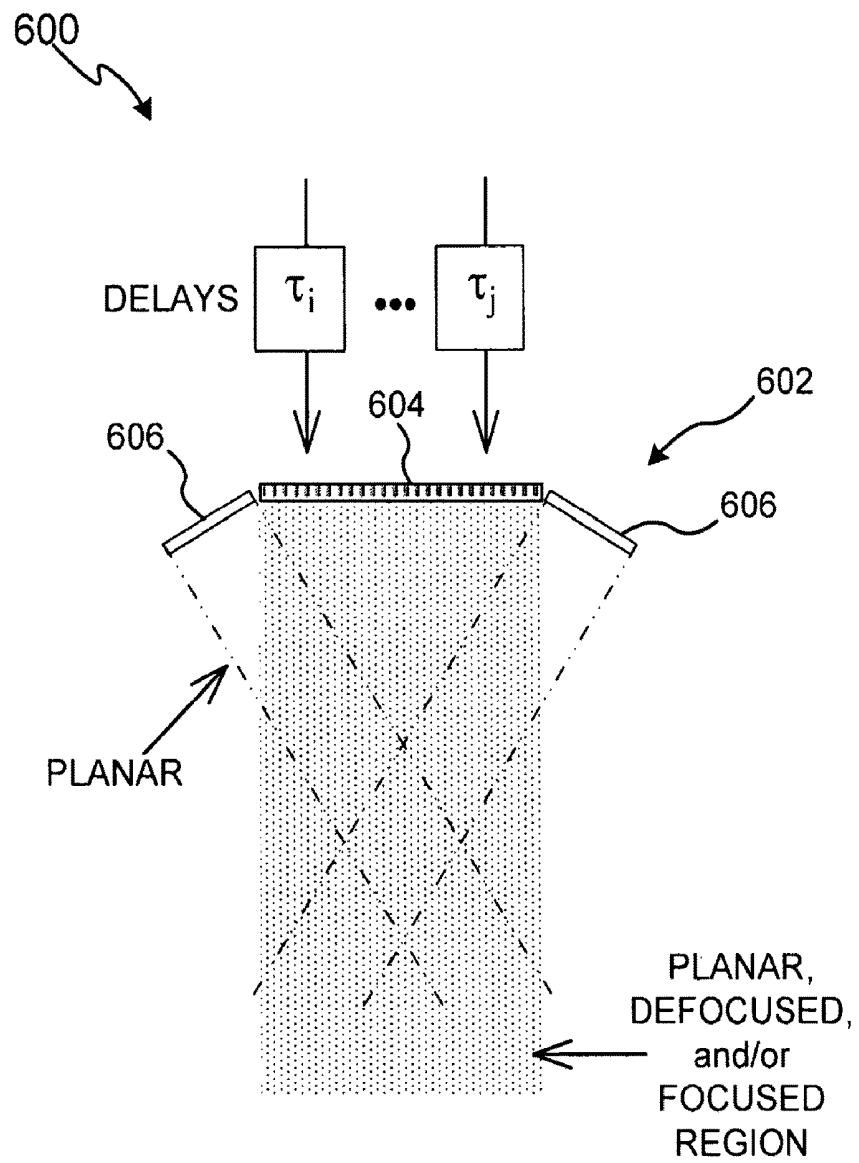


FIG. 5

**FIG. 6A**

**FIG. 6B**

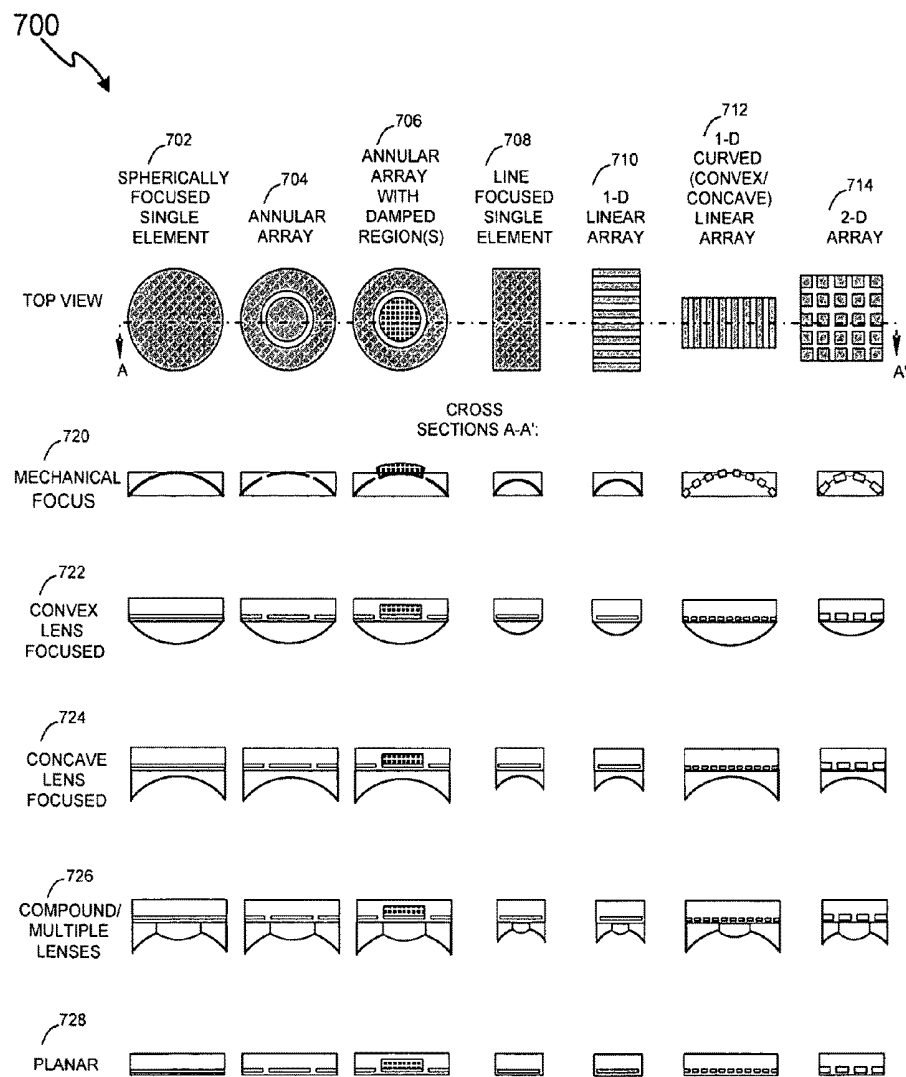


FIG. 7

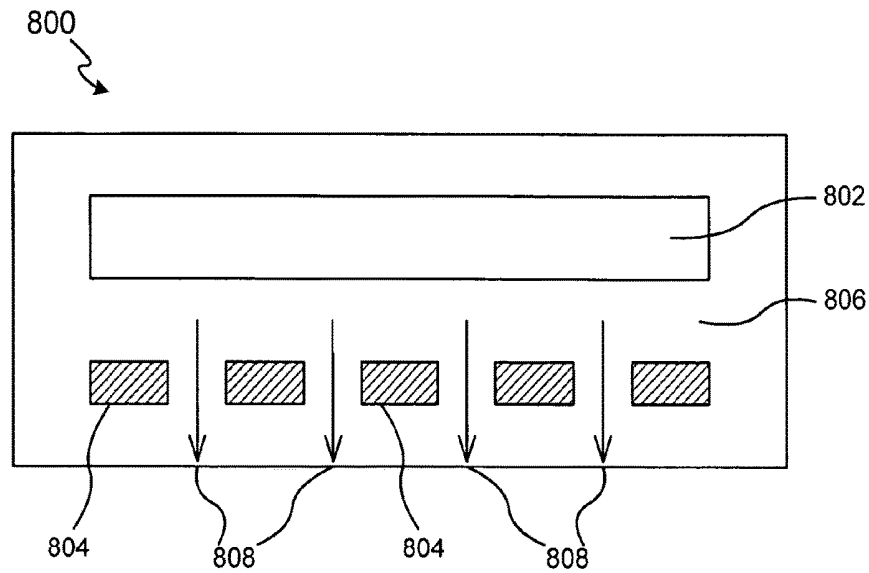


FIG. 8A

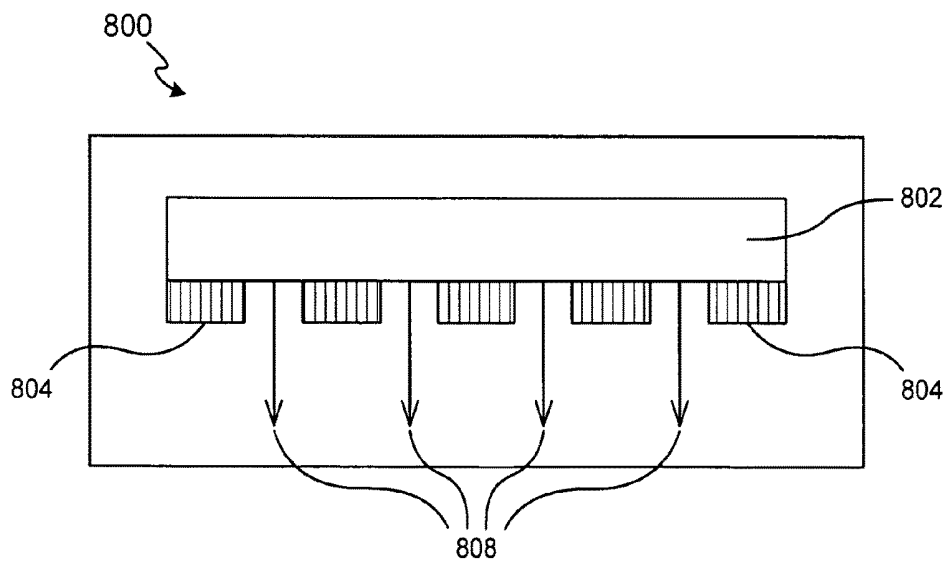


FIG. 8B

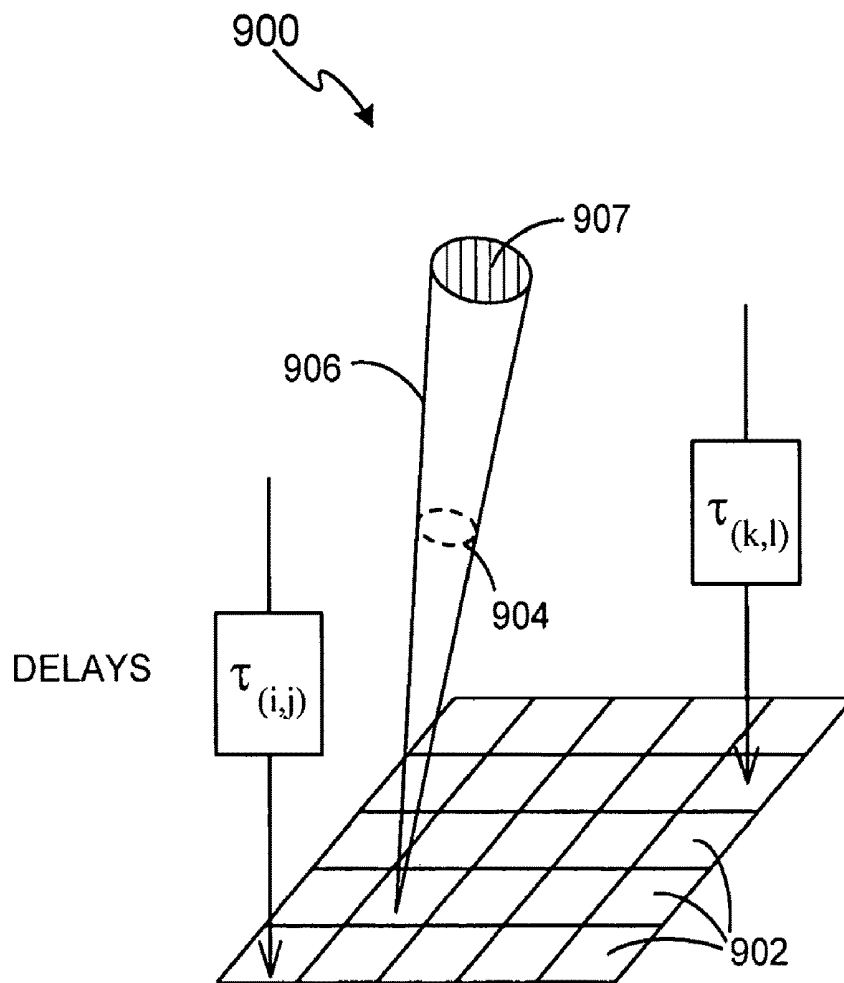


FIG. 9

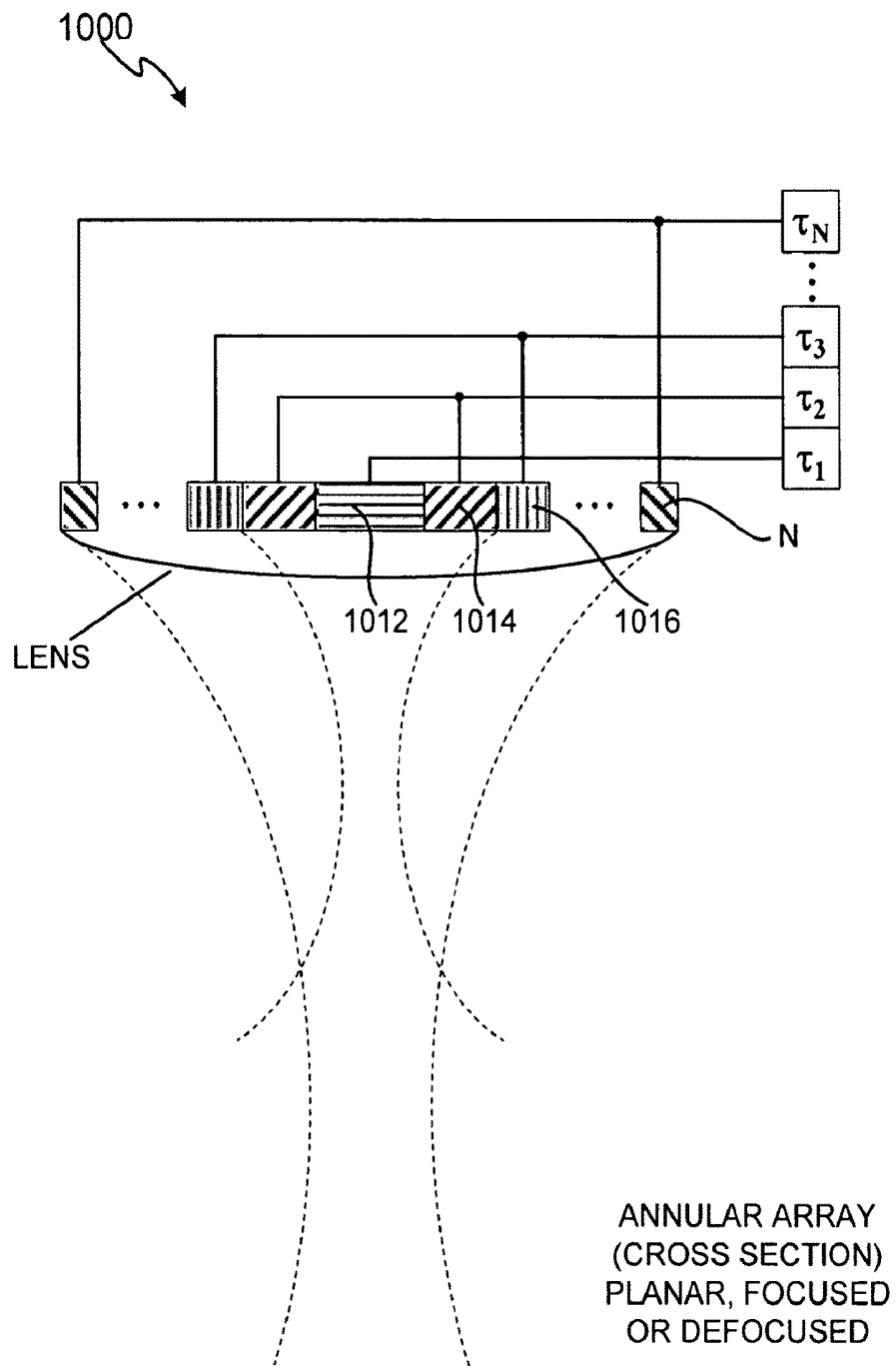
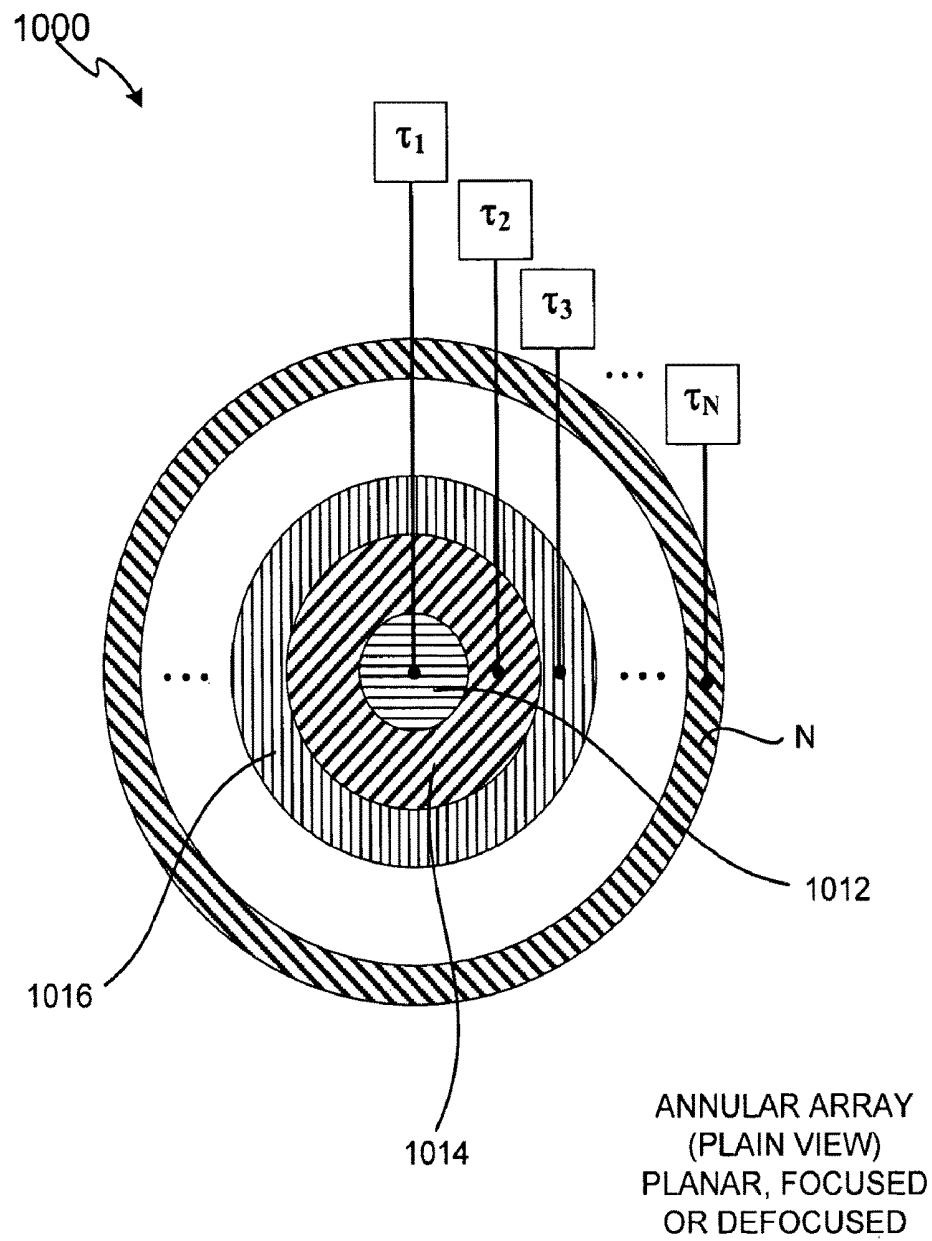


FIG. 10A

**FIG. 10B**

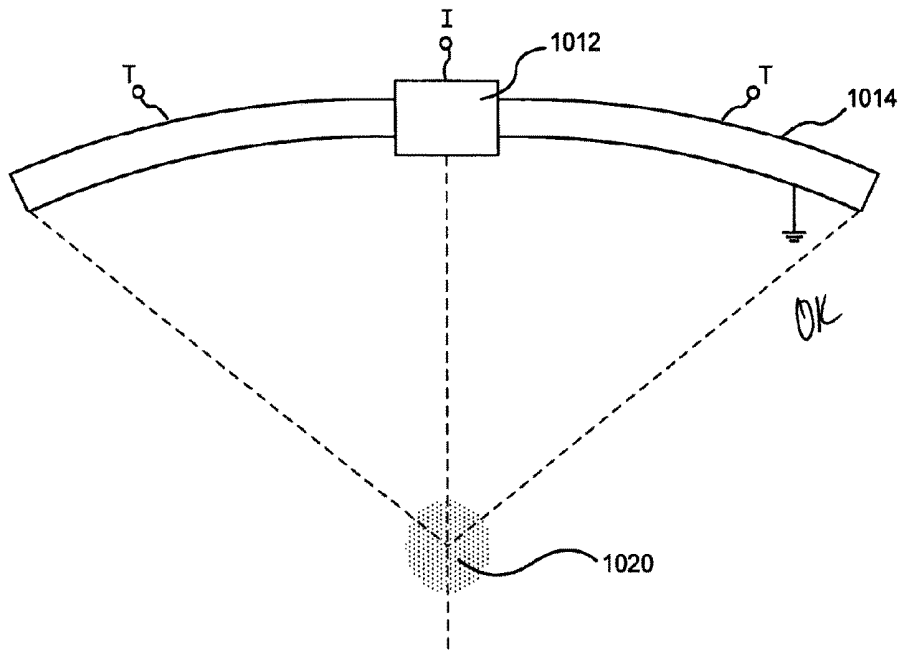


FIG. 10C

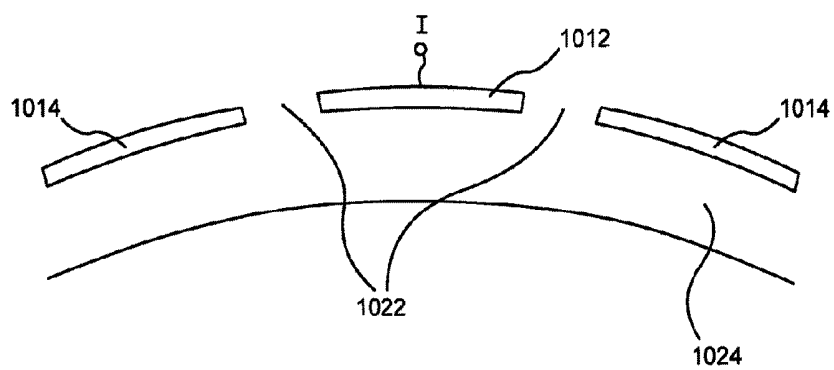


FIG. 10D

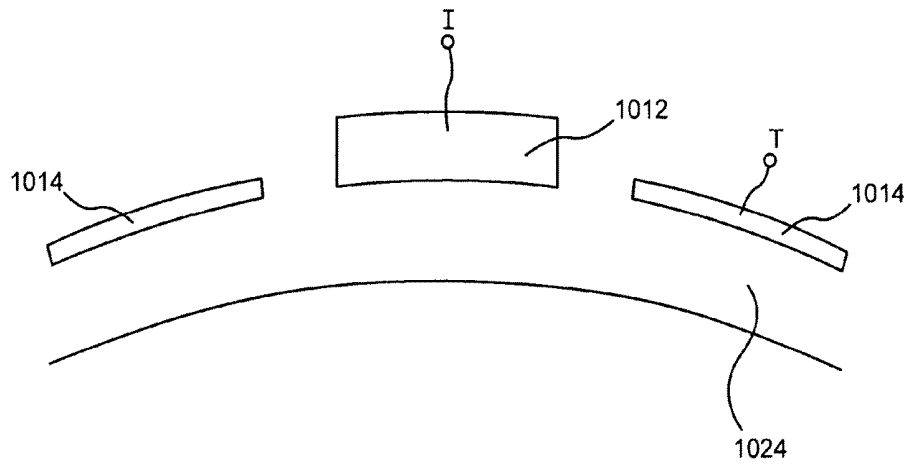


FIG. 10E

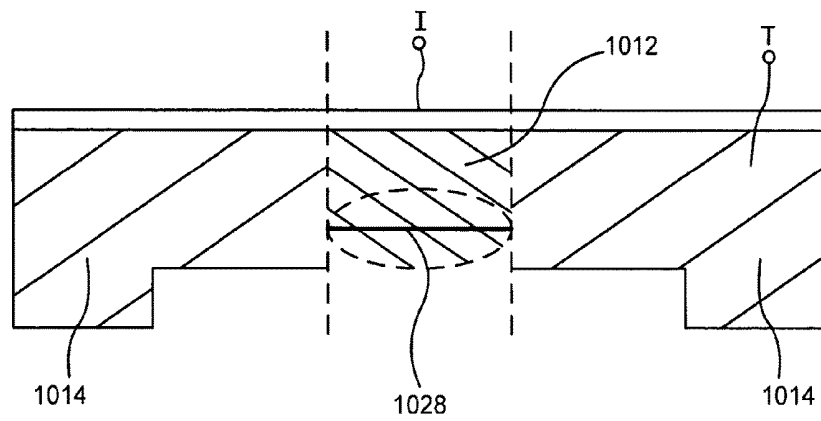


FIG. 10F

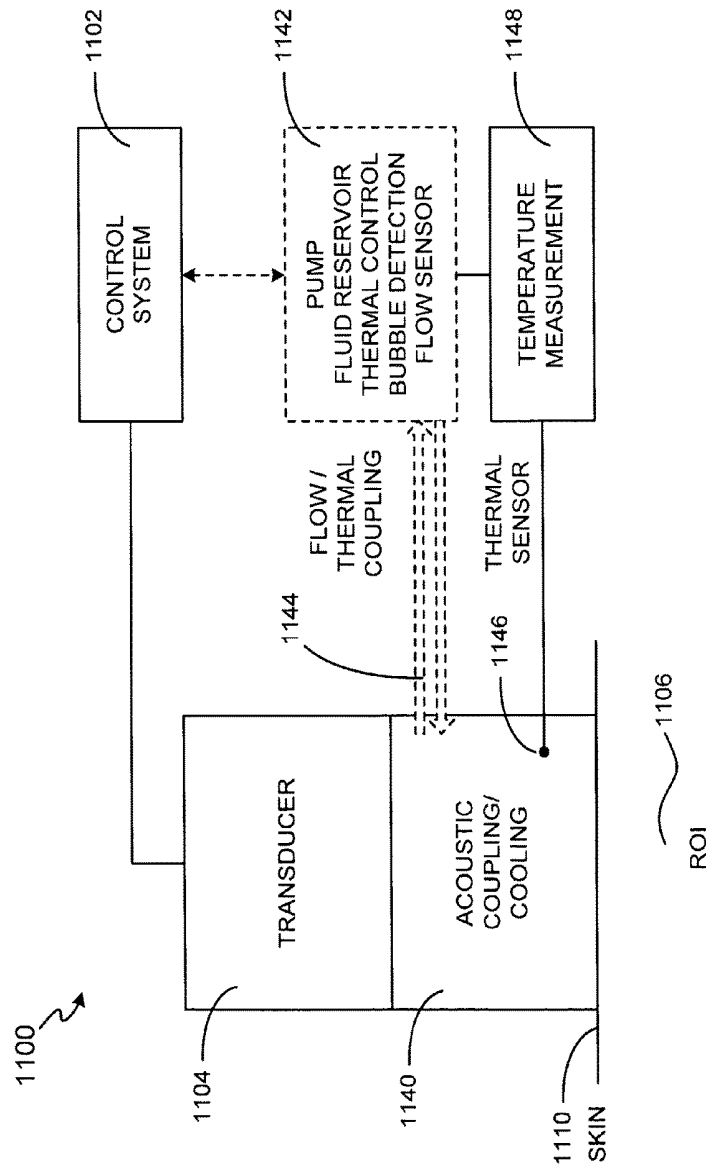
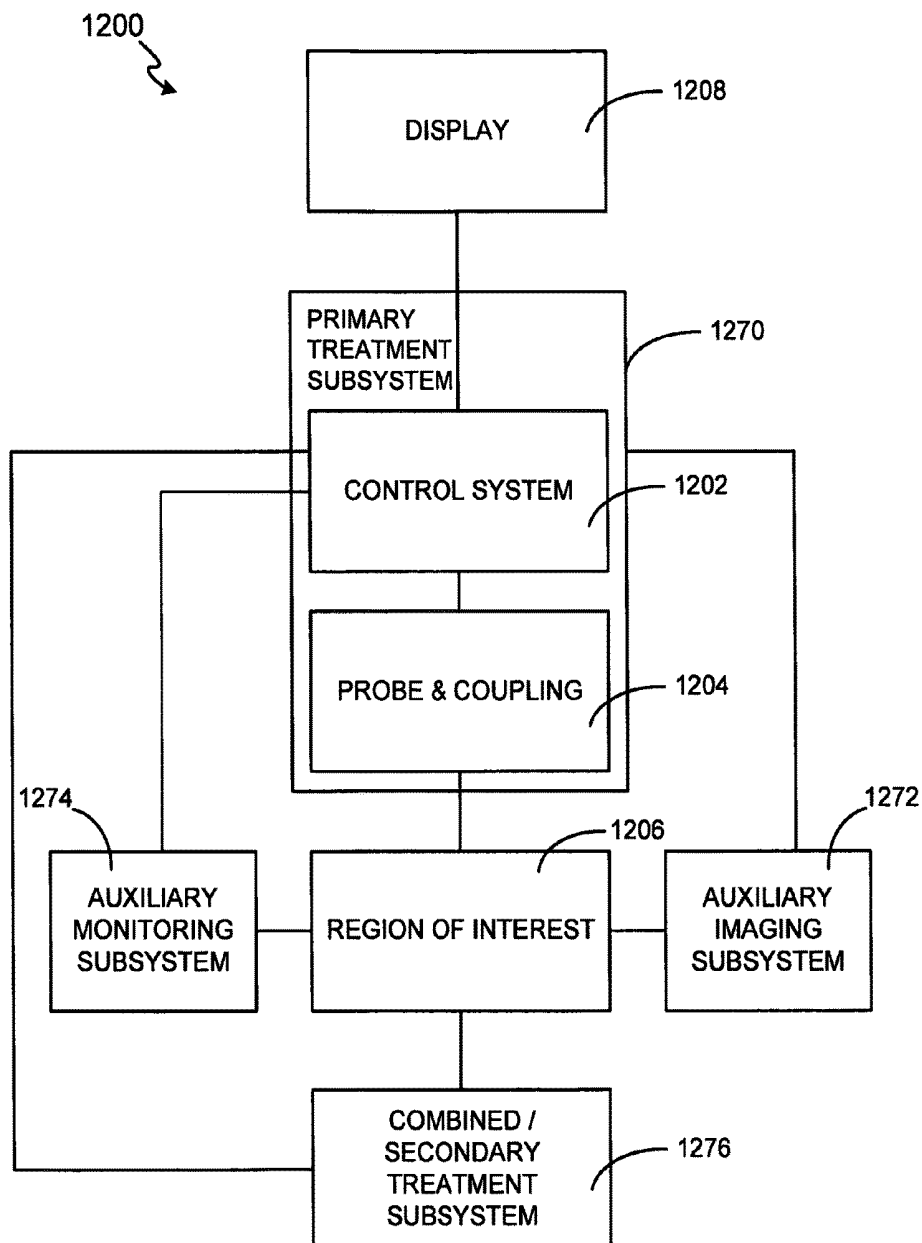
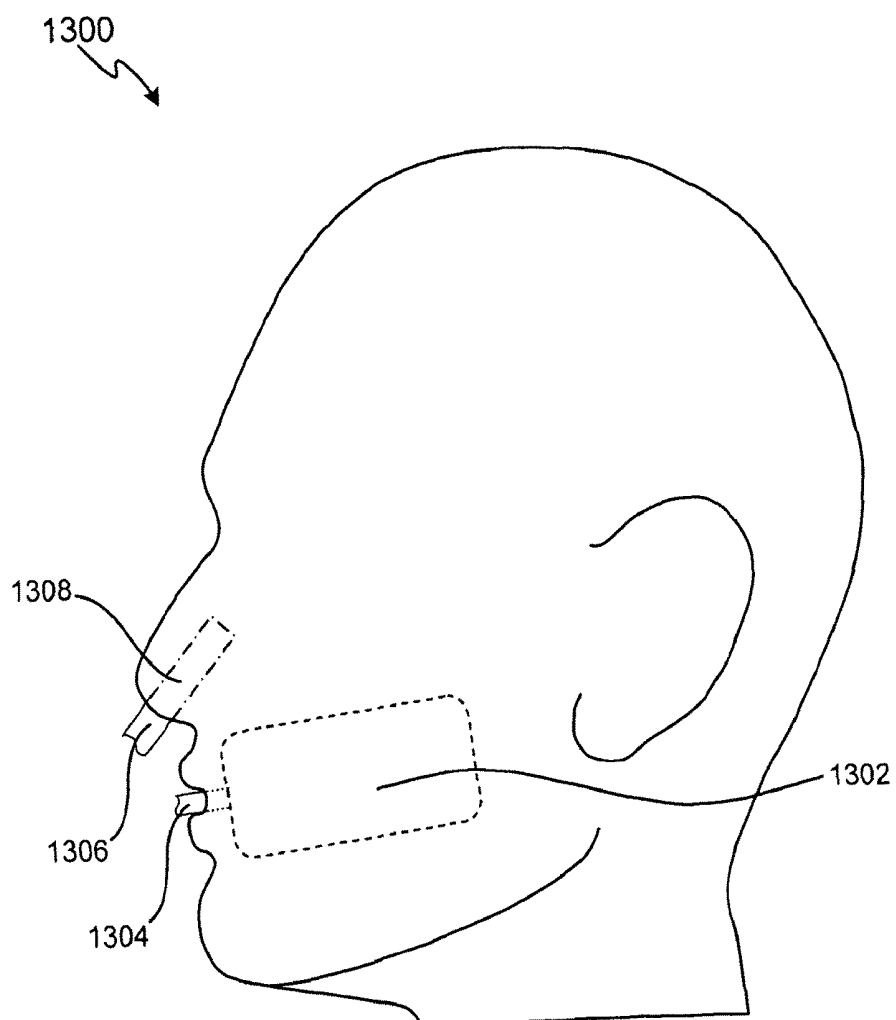


FIG. 11

**FIG. 12**

**FIG. 13**

ULTRASOUND PROBE FOR TREATING SKIN LAXITY

INCORPORATION BY REFERENCE TO ANY PRIORITY APPLICATIONS

This application is a continuation of U.S. patent application Ser. No. 15/821,070 issued as U.S. Pat. No. 10,010,724, which is a continuation of U.S. patent application Ser. No. 15/625,700, issued as U.S. Pat. No. 9,827,449, which is a continuation of U.S. patent application Ser. No. 15/248,407, issued as U.S. Pat. No. 9,694,211, which is a continuation of U.S. patent application Ser. No. 14/692,114, issued as U.S. Pat. No. 9,427,600, which is a continuation of U.S. patent application Ser. No. 14/169,709, issued as U.S. Pat. No. 9,039,619, which is a continuation of U.S. patent application Ser. No. 13/230,498, issued as U.S. Pat. No. 8,641,622, which is a continuation of U.S. patent application Ser. No. 11/163,150, issued as U.S. Pat. No. 8,066,641, which claims the benefit of priority to U.S. Provisional Application No. 60/617,295, each of which is incorporated in its entirety by reference herein. Any and all applications for which a foreign or domestic priority claim is identified in the Application Data Sheet as filed with the present application are hereby incorporated by reference under 37 CFR 1.57.

BACKGROUND

The present invention relates to ultrasound therapy and imaging systems, and in particular to a method and system for treating photoaged tissue.

Photoaging of human skin is a complex response due to inflammation, oxidative injury, cellular and extracellular changes induced by decades of sunlight exposure. UV wavelengths are thought to be mainly responsible. Both of the primary skin layers, epidermis and dermis, are affected. Epidermal photoaging includes pigmentary lesions called ephelides (freckles) and solar lentigines (larger pigmented spots), plus precancerous clonal lesions of keratinocytes called actinic keratoses. Thermal destruction of part or all of the epidermis, the outermost cellular layer of skin about 0.1 mm thick, is an effective treatment for epidermal photoaging. For example, lasers that vaporize epidermis are highly effective in a treatment called laser resurfacing. However laser resurfacing creates a significant skin wound with risk of infection, and prolonged healing. Dermal changes of photoaging include solar elastosis (an accumulation of abnormally-formed elastin fibers in the upper reticular layer of the dermis), laxity, loss of elasticity, fine and coarse wrinkles. Laser resurfacing to a depth below the dermoepidermal junction can be highly effective for improving dermal photoaging, through a process of stimulated wound healing. Deep chemical peels, dermabrasion and other methods of destruction of epidermis and/or dermis are also effective, and also produce a significant open skin wound with risk of infection and delayed healing.

Patterns of stimulated thermal damage to epidermis and/or dermis are also effective for treatment of photoaging. Recently, "fractional photothermolysis" using mid-infrared lasers to produce a microscopic array of thermal injury zones that include both epidermis and dermis was reported to be effective and well-tolerated for treatment of photoaging (D. Manstein et al. "Fractional Photothermolysis: a new concept for cutaneous remodeling using microscopic patterns of thermal injury." *Lasers Surg Med* 34:426-438, 2004). A primary advantage of fractional photothermolysis is that each zone of thermal injury is smaller than can be

easily seen with the unaided eye, and surrounded by a zone of healthy tissue that initiates a rapid healing response. As described Manstein, the epidermis is stimulated to heal rapidly and without creating an open wound. The microscopic zones of thermally injured epidermis slough harmlessly from the skin surface after several days to several weeks, leaving a rejuvenated epidermis with less photoaging changes. Repeat treatments, which are well tolerated, can be performed until a desired result is obtained. The microscopic zones of thermal injury with fractional photothermolysis extend well into the dermis, as well. Dermis does not heal as rapidly as epidermis, in general. Over weeks to months following treatment, some of the abnormal dermis due to photoaging is remodeled, however, leading to improvement in laxity, wrinkles and skin texture.

Fractional photothermolysis (FP) is intrinsically limited to regions of approximately the upper 1-millimeter of skin. The basic concept of producing well-controlled arrays of thermal injury is therefore limited with fractional photothermolysis, to superficial aspects of photoaging. Aging, which also causes laxity of the skin, and photoaging involve deeper layers of the dermis. Solar elastosis can extend throughout the dermis, to approximately 3 mm deep or more. Laxity and loss of elasticity due to aging are bulk problems of the dermis.

A fundamental requirement for producing arrays of small thermal injury zones using a source of radiant energy that propagates and is absorbed within tissue, is that the source of radiant energy be capable of being adequately delivered to the tissue depth for which the array is desired. Near the skin surface, light can be used, as in fractional photothermolysis. However, light that propagates more than about 1 mm through skin has been multiplied scattered, and can no longer be focused or delivered.

SUMMARY

A method and system for ultrasound treatment of photoaged tissue are provided. An exemplary method and system are configured for first, ultrasound imaging of the region of interest for localization of the treatment area, second, delivery of ultrasound energy at a depth and pattern to achieve the desired therapeutic effects, and third to monitor the treatment area during and after therapy to assess the results and/or provide feedback. The exemplary treatment method and system can be configured for producing arrays of sub-millimeter and larger zones of thermal ablation to treat the epidermal, superficial dermal, mid-dermal and deep dermal components of photoaged tissue.

In accordance with an exemplary embodiment, the treatment method and system use focused, unfocused, and/or defocused ultrasound for treatment of epidermal, superficial dermal, dermal, mid-dermal, and/or deep dermal components of photoaged tissue by adjusting the strength, depth, and/or type of focusing, energy levels and timing cadence. For example, focused ultrasound can be used to create precise arrays of microscopic thermal damage much deeper into the skin or even into subcutaneous structures. Detection of changes in the reflection of ultrasound can be used for feedback control to detect a desired effect on the tissue and used to control the exposure intensity, time, and/or position.

In accordance with an exemplary embodiment, an exemplary treatment system comprises an imaging/therapy probe, a control system and display system. The imaging/therapy probe can comprise various probe and/or transducer configurations. For example, the probe can be configured for a combined dual-mode imaging/therapy transducer, coupled

or co-housed imaging/therapy transducers, a separate therapy probe and imaging probe, or a single therapy probe. The control system and display system can also comprise various configurations for controlling probe and system functionality, including for example a microprocessor with software and a plurality of input/output and communication devices, a system for controlling electronic and/or mechanical scanning and/or multiplexing of transducers, a system for power delivery, systems for monitoring, systems for sensing the spatial position of the probe and/or temporal parameters of the transducers, and systems for handling user input and recording treatment input and results, among others.

BRIEF DESCRIPTION OF THE DRAWINGS

The subject matter of the invention is particularly pointed out in the concluding portion of the specification. The invention, however, both as to organization and method of operation, may best be understood by reference to the following description taken in conjunction with the accompanying drawing figures, in which like parts may be referred to by like numerals:

FIG. 1 illustrates a block diagram of a treatment system in accordance with an exemplary embodiment of the present invention;

FIGS. 2A-2D illustrates a schematic diagram of an ultrasound treatment system including therapy, imaging and/or monitoring and treating photoaged tissue in accordance with various exemplary embodiments of the present invention;

FIGS. 3A and 3B illustrate block diagrams of an exemplary control system in accordance with exemplary embodiments of the present invention;

FIGS. 4A and 4B illustrate block diagrams of an exemplary probe system in accordance with exemplary embodiments of the present invention;

FIG. 5 illustrates a cross-sectional diagram of an exemplary transducer in accordance with an exemplary embodiment of the present invention;

FIGS. 6A and 6B illustrate cross-sectional diagrams of an exemplary transducer in accordance with exemplary embodiments of the present invention;

FIG. 7 illustrates exemplary transducer configurations for ultrasound treatment in accordance with various exemplary embodiments of the present invention;

FIGS. 8A and 8B illustrate cross-sectional diagrams of an exemplary transducer in accordance with another exemplary embodiment of the present invention;

FIG. 9 illustrates an exemplary transducer configured as a two-dimensional, array for ultrasound treatment in accordance with an exemplary embodiment of the present invention;

FIGS. 10A-10F illustrate cross-sectional diagrams of exemplary transducers in accordance with other exemplary embodiments of the present invention;

FIG. 11 illustrates a schematic diagram of an acoustic coupling and cooling system in accordance with an exemplary embodiment of the present invention;

FIG. 12 illustrates a block diagram of an ultrasound treatment system combined with additional subsystems and methods of treatment monitoring and/or treatment imaging as well as a secondary treatment subsystem in accordance with an exemplary embodiment of the present invention; and

FIG. 13 illustrates a schematic diagram with imaging, therapy, or monitoring being provided with one or more

active or passive oral inserts in accordance with an exemplary embodiment of the present invention.

DETAILED DESCRIPTION

The present invention may be described herein in terms of various functional components and processing steps. It should be appreciated that such components and steps may be realized by any number of hardware components configured to perform the specified functions. For example, the present invention may employ various medical treatment devices, visual imaging and display devices, input terminals and the like, which may carry out a variety of functions under the control of one or more control systems or other control devices. In addition, the present invention may be practiced in any number of medical contexts and that the exemplary embodiments relating to a method and system for treating photoaged tissue as described herein are merely indicative of exemplary applications for the invention. For example, the principles, features and methods discussed may be applied to any medical application. Further, various aspects of the present invention may be suitably applied to other applications.

In accordance with various aspects of the present invention, a method and system for treating photoaged tissue are provided. For example, in accordance with an exemplary embodiment, with reference to FIG. 1, an exemplary treatment system **100** configured to treat a region of interest (ROI) **106** comprises a control system **102**, an imaging/therapy probe with acoustic coupling **104**, and a display system **108**. Control system **102** and display **108** can comprise various configurations for controlling functionality of probe **104** and system **100**, including for example a microprocessor with software and a plurality of input/output and communication devices, a system for controlling electronic and/or mechanical scanning and/or multiplexing of transducers, a system for power delivery, systems for monitoring, systems for sensing the spatial position of the probe and/or temporal parameters of the transducers, and/or systems for handling user input and recording treatment input and results, among others. Imaging/therapy probe **104** can comprise various probe and/or transducer configurations. For example, probe **104** can be configured for a combined dual-mode imaging/therapy transducer, coupled or co-housed imaging/therapy transducers, a separate therapy probe and separate imaging probe, or a single therapy probe. In accordance with exemplary embodiments, imaging transducers may operate at frequencies from approximately 2 to 75 MHz or more, while therapy energy can be delivered at frequencies from approximately 2 to 50 MHz, with 2 MHz to 25 MHz being typical.

For the treatment of photoaged tissue, it is desirable to be able to produce well controlled arrays of microscopic zones of thermal injury not only near the surface of skin, but in the mid-dermis, and/or in the deep dermis. Thermal ablation of dermis at temperatures greater than about 60° C., capable of producing denaturation of tissue, is also desirable in such arrays of thermal lesions. Shrinkage of dermis due to thermal action results from tightening of the skin.

In contrast to optical or RF approaches, ultrasound energy propagates as a wave with relatively little scattering, over depths up to many centimeters in tissue depending on the ultrasound frequency. The focal spot size achievable with any propagating wave energy, depends on wavelength. Ultrasound wavelength is equal to the acoustic velocity

divided by the ultrasound frequency. Attenuation (absorption, mainly) of ultrasound by tissue also depends on frequency.

In accordance with an exemplary embodiment, the use of focused, unfocused, or defocused ultrasound for treatment of epidermal, superficial dermal, dermal, middermal, and deep dermal components of photoaged tissue through adjustment of the strength, depth, and type of focusing, energy levels and timing cadence. For example, focused ultrasound can be used to create precise arrays of microscopic thermal ablation zones which have several advantages over fractional photothermolysis (FP). At high frequency and with superficial focusing or diffraction pattern, ultrasound ablation can mimic FP but utilize a simpler ablation device. Unlike fractional photothermolysis, ultrasound can produce an array of ablation zones much deeper into the skin or even into subcutaneous structures. Detection of changes in the reflection of ultrasound can be used for feedback control to detect a desired effect on the tissue and used to control the exposure intensity, time, and/or position.

To further illustrate the use of ultrasound for the treatment of photoaged tissue, with reference to FIG. 2A, an exemplary method and system are configured for initially imaging a region 222 of a region of interest 206 and displaying that region 224 during the localization of the treatment area and surrounding structures. After localization, delivery of ultrasound energy 220 at a depth, distribution, timing, and energy level to achieve the desired therapeutic effect of thermal ablation to treat an epidermis layer 212, superficial dermis layer 214, mid-dermis layer 216, and/or deep dermis layer 218 can be provided. Before, during, and after therapy, i.e., before, during, and after the delivery of ultrasound energy 220, exemplary method and system 200 can suitably monitor the treatment area and surrounding structures to plan and assess the results and/or provide feedback to control system 202 and/or a system user.

While an imaging function may be configured within control system 202 to facilitate imaging a region of interest, in accordance with another exemplary embodiment, an exemplary treatment system 200 may also be configured for therapy only or therapy and monitoring, without imaging functions. In such a case prior known depth of the region of interest, approximately 0 to 5 mm or less, is employed to achieve treatment zones in photoaged skin.

Probe 204 and/or transducers within can be mechanically and/or electronically scanned in a direction 226 to place treatment zones 260 over an extended area, such as a line to generate a matrix of closely spaced treatment spots. Treatment depth 220 can be adjusted between a range of approximately 0 to 5 mm, or otherwise until the depth of the deep dermis. Treatment may be confined to a fixed depth or a few discrete depths, or can be adjustment limited to a fine range, e.g. from approximately between 0 to 5 mm or the greatest depth of the deep dermis, or can be dynamically adjusted during treatment, to the treat region of interest 206 that lies above subcutaneous fat region 250.

In accordance with another exemplary embodiment of the present invention, with reference to FIG. 2B, a treated zone 260 may extend throughout regions of the dermis, and may even extend to the epidermis, 262. In addition, as a treated zone increases in depth its cross section may increase from small size 264 (sub millimeter) in a shallow region near or at the epidermis, to medium size 266 (sub millimeter to millimeter sized) in a middle zone near or at the mid dermis, to large size 268 (millimeter sized) in deep zones near or at the deep dermis. Furthermore a. single treated zone can have a shape expanding in cross section with depth, and/or be

composed of the fusion of several smaller treatment zones. Spacing of treatment zones can be on the order of the treatment zone size. The ultrasound beam can be spatially and/or temporally controlled by changing the position of the transducer, its frequency, treatment depth, drive amplitude, and timing via the control system. For example, the ultrasound beam can be controlled as set forth in U.S. patent application Ser. No. 11/163,148, filed Oct. 6, 2005, and entitled METHOD AND SYSTEM FOR CONTROLLED THERMAL INJURY OF HUMAN SUPERFICIAL TISSUE, and hereby incorporated by reference.

In accordance with another exemplary embodiment of the present invention, with reference to FIG. 2C, an exemplary treatment method and system 200 may be configured to monitor the temperature profile or other tissue parameters of region of interest 206, such as attenuation or speed of sound of the treatment region and suitably adjust the spatial and/or temporal characteristics and energy levels of the ultrasound therapy transducer. The results of such monitoring techniques may be indicated on display 208, such as through display of one-, two-, or three-dimensional images of monitoring results 270, or may comprise an indicator 272, such as a success, fail and/or completed/done type of indication, or combinations thereof. Additional treatment monitoring methods may be based on one or more of temperature, video, profilometry, strain imaging and/or gauges or any other suitable sensing method.

In accordance with another exemplary embodiment, with reference to FIG. 20, an expanded region of interest 280 can suitably include a combination of tissues, such as subcutaneous fat/adipose tissue 250. A combination of such tissues includes at least one of epidermis 212, superficial dermis 214, mid dermis 216, or deep dermis 218, in combination with at least one of muscle tissue, adipose tissue, or other tissues useful for treatment. For example, treatment 260 of superficial dermis may be performed in combination with treatment 220 of subcutaneous fat 250 by suitable adjustment of the spatial and temporal parameters of transducers in probe 204.

An exemplary control system 202 and display system 208 may be configured in various manners for controlling probe and system functionality for providing the various exemplary treatment methods illustrated above. For example, with reference to FIGS. 3A and 3B, in accordance with exemplary embodiments, an exemplary control system 300 can be configured for coordination and control of the entire therapeutic treatment process for producing arrays of sub-millimeter and larger zones of thermal ablation to treat the epidermal, superficial dermal, mid-dermal and deep dermal components of photoaged tissue. For example, control system 300 can suitably comprise power source components 302, sensing and monitoring components 304, cooling and coupling controls 306, and/or processing and control logic components 308. Control system 300 can be configured and optimized in a variety of ways with more or less subsystems and components to implement the therapeutic system for controlled thermal injury of photoaged tissue, and the embodiments in FIGS. 3A and 3B are merely for illustration purposes.

For example, for power sourcing components 302, control system 300 can comprise one or more direct current (DC) power supplies 303 configured to provide electrical energy for entire control system 300, including power required by a transducer electronic amplifier/driver 312. A DC current sense device 305 can also be provided to confirm the level of power going into amplifiers/drivers 312 for safety and monitoring purposes.

Amplifiers/drivers **312** can comprise multi-channel or single channel power amplifiers and/or drivers. In accordance with an exemplary embodiment for transducer array configurations, amplifiers/drivers **312** can also be configured with a beamformer to facilitate array focusing. An exemplary beamformer can be electrically excited by an oscillator/digitally controlled waveform synthesizer **310** with related switching logic.

The power sourcing components can also include various filtering configurations **314**. For example, switchable harmonic filters and/or matching may be used at the output of amplifier/driver **312** to increase the drive efficiency and effectiveness. Power detection components **316** may also be included to confirm appropriate operation and calibration. For example, electric power and other energy detection components **316** may be used to monitor the amount of power going to an exemplary probe system.

Various sensing and monitoring components **304** may also be suitably implemented within control system **300**. For example, in accordance with an exemplary embodiment, monitoring, sensing and interface control components **324** may be configured to operate with various motion detection systems implemented within transducer probe **204** to receive and process information such as acoustic or other spatial and temporal information from a region of interest. Sensing and monitoring components can also include various controls, interfacing and switches **309** and/or power detectors **316**. Such sensing and monitoring components **304** can facilitate open-loop and/or closed-loop feedback systems within treatment system **200**.

Cooling/coupling control systems **306** may be provided to remove waste heat from an exemplary probe **204**, provide a controlled temperature at the superficial tissue interface and deeper into tissue, and/or provide acoustic coupling from transducer probe **204** to region-of-interest **206**. Such cooling/coupling control systems **306** can also be configured to operate in both open-loop and/or closed-loop feedback arrangements with various coupling and feedback components.

Processing and control logic components **308** can comprise various system processors and digital control logic **307**, such as one or more of microcontrollers, microprocessors, field-programmable gate arrays (FPGAs), computer boards, and associated components, including firmware and control software **326**, which interfaces to user controls and interfacing circuits as well as input/output circuits and systems for communications, displays, interfacing, storage, documentation, and other useful functions. System software and firmware **326** controls all initialization, timing, level setting, monitoring, safety monitoring, and all other system functions required to accomplish user-defined treatment objectives. Further, various control switches **308** can also be suitably configured to control operation.

An exemplary transducer probe **204** can also be configured in various manners and comprise a number of reusable and/or disposable components and parts in various embodiments to facilitate its operation. For example, transducer probe **204** can be configured within any type of transducer probe housing or arrangement for facilitating the coupling of transducer to a tissue interface, with such housing comprising various shapes, contours and configurations. Transducer probe **204** can comprise any type of matching, such as for example, electric matching, which may be electrically switchable; multiplexer circuits and/or aperture/element selection circuits; and/or probe identification devices, to certify probe handle, electric matching, transducer usage history and calibration, such as one or more serial EEPROM

(memories). Transducer probe **204** may also comprise cables and connectors; motion mechanisms, motion sensors and encoders; thermal monitoring sensors; and/or user control and status related switches, and indicators such as LEDs. For example, a motion mechanism in probe **204** may be used to controllably create multiple lesions, or sensing of probe motion itself may be used to controllably create multiple lesions and/or stop creation of lesions, e.g. for safety reasons if probe **204** is suddenly jerked or is dropped. In addition, an external motion encoder arm may be used to hold the probe during use, whereby the spatial position and attitude of probe **104** is sent to the control system to help controllably create lesions. Furthermore, other sensing functionality such as profilometers or other imaging modalities may be integrated into the probe in accordance with various exemplary embodiments.

With reference to FIGS. **4A** and **4B**, in accordance with an exemplary embodiment, a transducer probe **400** can comprise a control interface **402**, a transducer **404**, coupling components **406**, and monitoring/sensing components **408**, and/or motion mechanism **410**. However, transducer probe **400** can be configured and optimized in a variety of ways with more or less parts and components to provide ultrasound energy for controlled thermal injury of photoaged tissue, and the embodiments in FIGS. **4A** and **4B** are merely for illustration purposes.

Control interface **402** is configured for interfacing with control system **300** to facilitate control of transducer probe **400**. Control interface components **402** can comprise multiplexer/aperture select **424**, switchable electric matching networks **426**, serial EEPROMs and/or other processing components and matching and probe usage information **430** and interface connectors **432**.

Coupling components **406** can comprise various devices to facilitate coupling of transducer probe **400** to a region of interest. For example, coupling components **406** can comprise cooling and acoustic coupling system **420** configured for acoustic coupling of ultrasound energy and signals. Acoustic cooling/coupling system **420** with possible connections such as manifolds may be utilized to couple sound into the region-of-interest, control temperature at the interface and deeper into tissue, provide liquid-filled lens focusing, and/or to remove transducer waste heat. Coupling system **420** may facilitate such coupling through use of various coupling mediums, including air and other gases, water and other fluids, gels, solids, and/or any combination thereof, or any other medium that allows for signals to be transmitted between transducer active elements **412** and a region of interest. In addition to providing a coupling function, in accordance with an exemplary embodiment, coupling system **420** can also be configured for providing temperature control during the treatment application. For example, coupling system **420** can be configured for controlled cooling of an interface surface or deeper region between transducer probe **400** and a region of interest and beyond by suitably controlling the temperature of the coupling medium. The suitable temperature for such coupling medium can be achieved in various manners, and utilize various feedback systems, such as thermocouples, thermistors or any other device or system configured for temperature measurement of a coupling medium. Such controlled cooling can be configured to further facilitate spatial and/or thermal energy delivery control of transducer probe **400**.

In accordance with an exemplary embodiment, with additional reference to FIG. **11**, acoustic coupling and cooling **1140** can be provided to acoustically couple energy and imaging signals from transducer probe **1104** to and from the

region of interest **1102**, to provide thermal control at the probe to region-of-interest interface **1110** and deeper into tissue, and to remove potential waste heat from the transducer probe at region **1144**. Temperature monitoring can be provided at the coupling interface via a thermal sensor **1146** to provide a mechanism of temperature measurement **1148** and control via control system **1106** and a thermal control system **1142**. Thermal control may consist of passive cooling such as via heat sinks or natural conduction and convection or via active cooling such as with peltier thermoelectric coolers, refrigerants, or fluid-based systems comprised of pump, fluid reservoir, bubble detection, flow sensor, flow channels/tubing **1144** and thermal control **1142**.

With continued reference to FIG. 4, monitoring and sensing components **408** can comprise various motion and/or position sensors **416**, temperature monitoring sensors **418**, user control and feedback switches **414** and other like components for facilitating control by control system **300**, e.g., to facilitate spatial and/or temporal control through open-loop and closed-loop feedback arrangements that monitor various spatial and temporal characteristics.

Motion mechanism **410** can comprise manual operation, mechanical arrangements, or some combination thereof. For example, a motion mechanism **422** can be suitably controlled by control system **300**, such as through the use of accelerometers, encoders or other position/orientation devices **416** to determine and enable movement and positions of transducer probe **400**. Linear, rotational or variable movement can be facilitated, e.g., those depending on the treatment application and tissue contour surface.

Transducer **404** can comprise one or more transducers configured for treating of SMAS layers and targeted regions. Transducer **404** can also comprise one or more transduction elements and/or lenses **412**. The transduction elements can comprise a piezoelectrically active material, such as lead zirconate titanate (PZT), or any other piezoelectrically active material, such as a piezoelectric ceramic, crystal, plastic, and/or composite materials, as well as lithium niobate, lead titanate, barium titanate, and/or lead metaniobate. In addition to, or instead of, a piezoelectrically active material, transducer **404** can comprise any other materials configured for generating radiation and/or acoustical energy. Transducer **404** can also comprise one or more matching layers configured along with the transduction element such as coupled to the piezoelectrically active material. Acoustic matching layers and/or damping may be employed as necessary to achieve the desired electroacoustic response.

In accordance with an exemplary embodiment, the thickness of the transduction element of transducer **404** can be configured to be uniform. That is, a transduction element **412** can be configured to have a thickness that is substantially the same throughout. In accordance with another exemplary embodiment, the thickness of a transduction element **412** can also be configured to be variable. For example, transduction element(s) **412** of transducer **404** can be configured to have a first thickness selected to provide a center operating frequency of approximately 2 kHz to 75 MHz, such as for imaging applications. Transduction element **412** can also be configured with a second thickness selected to provide a center operating frequency of approximately 2 to 50 MHz, and typically between 2 MHz and 25 MHz for therapy application. Transducer **404** can be configured as a single broadband transducer excited with at least two or more frequencies to provide an adequate output for generating a desired response. Transducer **404** can also be configured as two or more individual transducers, wherein each transducer comprises one or more transduction ele-

ment. The thickness of the transduction elements can be configured to provide center-operating frequencies in a desired treatment range.

Transducer **404** may be composed of one or more individual transducers in any combination of focused, planar, or unfocused single-element, multi-element, or array transducers, including 1-D, 2-D, and annular arrays; linear, curvilinear, sector, or spherical arrays; spherically, cylindrically, and/or electronically focused, defocused, and/or lensed sources. For example, with reference to an exemplary embodiment depicted in FIG. 5, transducer **500** can be configured as an acoustic array **502** to facilitate phase focusing. That is, transducer **500** can be configured as an array of electronic apertures that may be operated by a variety of phases via variable electronic time delays. By the term "operated," the electronic apertures of transducer **500** may be manipulated, driven, used, and/or configured to produce and/or deliver an energy beam corresponding to the phase variation caused by the electronic time delay. For example, these phase variations can be used to deliver defocused beams **508**, planar beams **504**, and/or focused beams **506**, each of which may be used in combination to achieve different physiological effects in a region of interest **510**. Transducer **500** may additionally comprise any software and/or other hardware for generating, producing and/or driving a phased aperture array with one or more electronic time delays.

Transducer **500** can also be configured to provide focused treatment to one or more regions of interest using various frequencies. In order to provide focused treatment, transducer **500** can be configured with one or more variable depth devices to facilitate treatment. For example, transducer **500** may be configured with variable depth devices disclosed in U.S. patent application Ser. No. 10/944,500, entitled "System and Method for Variable Depth Ultrasound", filed on Sep. 16, 2004, having at least one common inventor and a common Assignee as the present application, and incorporated herein by reference. In addition, transducer **500** can also be configured to treat one or more additional ROI **510** through the enabling of sub-harmonics or pulseecho imaging, as disclosed in U.S. patent application Ser. No. 10/944,499, entitled "Method and System for Ultrasound Treatment with a Multi-directional Transducer," filed on Sep. 16, 2004, having at least one common inventor and a common Assignee as the present application, and also incorporated herein by reference.

Moreover, any variety of mechanical lenses or variable focus lenses, e.g. liquid-filled lenses, may also be used to focus and/or defocus the sound field. For example, with reference to exemplary embodiments depicted in FIGS. 6A and 6B, transducer **600** may also be configured with an electronic focusing array **604** in combination with one or more transduction elements **606** to facilitate increased flexibility in treating ROI **610**. Array **604** may be configured in a manner similar to transducer **502**. That is, array **604** can be configured as an array of electronic apertures that may be operated by a variety of phases via variable electronic time delays, for example, T1, T2 . . . Tj. By the term "operated," the electronic apertures of array **604** may be manipulated, driven, used, and/or configured to produce and/or deliver energy in a manner corresponding to the phase variation caused by the electronic time delay. For example, these phase variations can be used to deliver defocused beams, planar beams, and/or focused beams, each of which may be used in combination to achieve different physiological effects in ROI **610**.

Transduction elements **606** may be configured to be concave, convex, and/or planar. For example, in an exemplary embodiment depicted in FIG. **6A**, transduction elements **606** are configured to be concave in order to provide focused energy for treatment of ROI **610**. Additional embodiments are disclosed in U.S. patent application Ser. No. 10/944,500, entitled "Variable Depth Transducer System and Method", and again incorporated herein by reference.

In another exemplary embodiment, depicted in FIG. **68**, transduction elements **606** can be configured to be substantially flat in order to provide substantially uniform energy to ROI **610**. While FIGS. **6A** and **68** depict exemplary embodiments with transduction elements **604** configured as concave and substantially flat, respectively, transduction elements **604** can be configured to be concave, convex, and/or substantially flat. In addition, transduction elements **604** can be configured to be any combination of concave, convex, and/or substantially flat structures. For example, a first transduction element can be configured to be concave, while a second transduction element can be configured to be substantially flat.

With reference to FIGS. **8A** and **8B**, transducer **404** can be configured as single-element arrays, wherein a single-element **802**, e.g., a transduction element of various structures and materials, can be configured with a plurality of masks **804**, such masks comprising ceramic, metal or any other material or structure for masking or altering energy distribution from element **802**, creating an array of energy distributions **808**. Masks **804** can be coupled directly to element **802** or separated by a standoff **806**, such as any suitably solid or liquid material.

An exemplary transducer **404** can also be configured as an annular array to provide planar, focused and/or defocused acoustical energy. For example, with reference to FIGS. **10A** and **10B**, in accordance with an exemplary embodiment, an annular array **1000** can comprise a plurality of rings **1012**, **1014**, **1016** to N. Rings **1012**, **1014**, **1016** to N can be mechanically and electrically isolated into a set of individual elements, and can create planar, focused, or defocused waves. For example, such waves can be centered on-axis, such as by methods of adjusting corresponding transmit and/or receive delays, T1, T2, T3 . . . TN. An electronic focus can be suitably moved along various depth positions, and can enable variable strength or beam tightness, while an electronic defocus can have varying amounts of defocusing. In accordance with an exemplary embodiment, a lens and/or convex or concave shaped annular array **1000** can also be provided to aid focusing or defocusing such that any time differential delays can be reduced. Movement of annular array **800** in one, two or three-dimensions, or along any path, such as through use of probes and/or any conventional robotic arm mechanisms, may be implemented to scan and/or treat a volume or any corresponding space within a region of interest.

Transducer **404** can also be configured in other annular or non-array configurations for imaging/therapy functions. For example, with reference to FIGS. **10C-10F**, a transducer can comprise an imaging element **1012** configured with therapy element(s) **1014**. Elements **1012** and **1014** can comprise a single-transduction element, e.g., a combined imaging/transducer element, or separate elements, can be electrically isolated **1022** within the same transduction element or between separate imaging and therapy elements, and/or can comprise standoff **1024** or other matching layers, or any combination thereof. For example, with particular reference to FIG. **10F**, a transducer can comprise an imaging element

1012 having a surface **1028** configured for focusing, defocusing or planar energy distribution, with therapy elements **1014** including a stepped-configuration lens configured for focusing, defocusing, or planar energy distribution.

In accordance with various exemplary embodiments of the present invention, transducer **404** may be configured to provide one, two and/or three-dimensional treatment applications for focusing acoustic energy to one or more regions of interest. For example, as discussed above, transducer **404** can be suitably diced to form a one-dimensional array, e.g., transducer **602** comprising a single array of sub-transduction elements.

In accordance with another exemplary embodiment, transducer **404** may be suitably diced in two-dimensions to form a two-dimensional array. For example, with reference to FIG. **9**, an exemplary two-dimensional array **900** can be suitably diced into a plurality of two-dimensional portions **902**. Two-dimensional portions **902** can be suitably configured to focus on the treatment region at a certain depth, and thus provide respective slices **904**, **907** of the treatment region. As a result, the two-dimensional array **900** can provide a two-dimensional slicing of the image plane of a treatment region, thus providing two-dimensional treatment.

In accordance with another exemplary embodiment, transducer **404** may be suitably configured to provide three-dimensional treatment. For example, to provide three-dimensional treatment of a region of interest, with reference again to FIG. **1**, a three-dimensional system can comprise a transducer within probe **104** configured with an adaptive algorithm, such as, for example, one utilizing three-dimensional graphic software, contained in a control system, such as control system **102**. The adaptive algorithm is suitably configured to receive two-dimensional imaging, temperature and/or treatment or other tissue parameter information relating to the region of interest, process the received information, and then provide corresponding three-dimensional imaging, temperature and/or treatment information.

In accordance with an exemplary embodiment, with reference again to FIG. **9**, an exemplary three-dimensional system can comprise a two-dimensional array **900** configured with an adaptive algorithm to suitably receive **904** slices from different image planes of the treatment region, process the received information, and then provide volumetric information **906**, e.g., three-dimensional imaging, temperature and/or treatment information. Moreover, after processing the received information with the adaptive algorithm, the two-dimensional array **900** may suitably provide therapeutic heating to the volumetric region **906** as desired.

In accordance with other exemplary embodiments, rather than utilizing an adaptive algorithm, such as three-dimensional software, to provide three-dimensional imaging and/or temperature information, an exemplary three-dimensional system can comprise a single transducer **404** configured within a probe arrangement to operate from various rotational and/or translational positions relative to a target region.

To further illustrate the various structures for transducer **404**, with reference to FIG. **7**, ultrasound therapy transducer **700** can be configured for a single focus, an array of foci, a locus of foci, a line focus, and/or diffraction patterns. Transducer **700** can also comprise single elements, multiple elements, annular arrays, one-, two-, or three-dimensional arrays, broadband transducers, and/or combinations thereof, with or without lenses, acoustic components, and mechanical and/or electronic focusing. Transducers configured as spherically focused single elements **702**, annular arrays **704**, annular arrays with damped regions **706**, line focused single

elements **708**, 1-0 linear arrays **710**, 1-0 curvilinear arrays in concave or convex form, with or without elevation focusing, 2-D arrays, and 3-D spatial arrangements of transducers may be used to perform therapy and/or imaging and acoustic monitoring functions. For any transducer configuration, focusing and/or defocusing may be in one plane or two planes via mechanical focus **720**, convex lens **722**, concave lens **724**, compound or multiple lenses **726**, planar form **728**, or stepped form, such as illustrated in FIG. 10F. Any transducer or combination of transducers may be utilized for treatment. For example, an annular transducer may be used with an outer portion dedicated to therapy and the inner disk dedicated to broadband imaging wherein such imaging transducer and therapy transducer have different acoustic lenses and design, such as illustrated in FIG. 1 OC-1 OF.

Moreover, such transduction elements **700** may comprise a piezoelectrically active material, such as lead zirconate titanate (PZT), or any other piezoelectrically active material, such as a piezoelectric ceramic, crystal, plastic, and/or composite materials, as well as lithium niobate, lead titanate, barium titanate, and/or lead metaniobate. Transduction elements **700** may also comprise one or more matching layers configured along with the piezoelectrically active material. In addition to or instead of piezoelectrically active material, transduction elements **700** can comprise any other materials configured for generating radiation and/or acoustical energy. A means of transferring energy to and from the transducer to the region of interest is provided.

In accordance with another exemplary embodiment, with reference to FIG. 12, an exemplary treatment system **200** can be configured with and/or combined with various auxiliary systems to provide additional functions. For example, an exemplary treatment system **1200** for treating a region of interest **1202** can comprise a control system **1206**, a probe **1204**, and a display **1208**. Treatment system **1200** further comprises an auxiliary imaging modality **1272** and/or auxiliary monitoring modality **1274** may be based upon at least one of photography and other visual optical methods, magnetic resonance imaging (MRI), computed tomography (CT), optical coherence tomography (OCT), electromagnetic, microwave, or radio frequency (RF) methods, positron emission tomography (PET), infrared, ultrasound, acoustic, or any other suitable method of visualization, localization, or monitoring of epidermal, superficial dermal, mid-dermal and deep dermal components within the region-of-interest **1202**, including imaging/monitoring enhancements. Such imaging/monitoring enhancement for ultrasound imaging via probe **1204** and control system **1206** could comprise M-mode, persistence, filtering, color, Doppler, and harmonic imaging among others; furthermore an ultrasound treatment system **1270**, as a primary source of treatment, may be combined with a secondary source of treatment **1276**, including radio frequency (RF), intense pulsed light (IPL), laser, infrared laser, microwave, or any other suitable energy source.

In accordance with another exemplary embodiment, with reference to FIG. 13, treatment composed of imaging, monitoring, and/or therapy to a region of interest **1302** and/or **1308** may be aided, augmented, and/or delivered with passive or active devices **1304** and/or **1306** within the oral and/or nasal cavity, respectively. For example, if passive or active device **1304** and/or **1306** are second transducers or acoustic reflectors acoustically coupled to the mucous membranes it is possible to obtain through transmission, tomographic, or round-trip acoustic waves which are useful for treatment monitoring, such as in measuring acoustic speed of sound and attenuation, which are temperature dependent;

furthermore such transducers could be used to treat and/or image. In addition an active, passive, or active/passive object **1304** and/or **1306** may be used to flatten the skin, and/or may be used as an imaging grid, marker, or beacon, to aid determination of position. A passive or active device **1304** and/or **1306** may also be used to aid cooling or temperature control. Natural air in the oral cavity and/or nasal cavity may also be used as passive device **1304** and/or **1306** whereby it may be utilized to as an acoustic reflector to aid thickness measurement and monitoring function.

The present invention has been described above with reference to various exemplary embodiments. However, those skilled in the art will recognize that changes and modifications may be made to the exemplary embodiments without departing from the scope of the present invention. For example, the various operational steps, as well as the components for carrying out the operational steps, may be implemented in alternate ways depending upon the particular application or in consideration of any number of cost functions associated with the operation of the system, e.g., various of the steps may be deleted, modified, or combined with other steps. These and other changes or modifications are intended to be included within the scope of the present invention, as set forth in the following claims.

What is claimed is:

1. An ultrasound probe for treatment of skin laxity, the ultrasound probe comprising:

a housing, wherein inside the housing comprises a motion mechanism and an ultrasound transducer,

wherein the ultrasound transducer comprises a single active focused piezoelectric ultrasound therapy element,

wherein the piezoelectric ultrasound therapy element is configured to provide a single mechanical focus configured to provide ultrasound therapy energy in a form of a single thermal focus in a tissue at one or more depths below a skin surface to treat the tissue,

wherein the tissue comprises any of the group consisting of: an epidermal tissue, a superficial dermal tissue, a mid-dermal tissue, a deep dermal tissue, a muscle tissue, and an adipose tissue,

wherein a portion of the housing is configured for acoustic coupling to the skin surface;

wherein the piezoelectric ultrasound therapy element is configured for delivery of energy at a temperature sufficient to tighten at least a portion of the tissue at the one or more depths under the skin surface,

wherein the single mechanical focus is formed without electronic focusing and without a lens,

wherein the piezoelectric ultrasound therapy element is connected to the motion mechanism,

wherein the motion mechanism is configured to operate with an encoder, wherein the motion mechanism is configured to move the piezoelectric ultrasound therapy element to form a plurality of thermal lesions at the one or more depths for tightening at least a portion of the tissue for reducing skin laxity.

2. The ultrasound probe of claim 1, wherein the ultrasound probe is disposable,

wherein the single thermal focus is one of the group consisting of: a spherical focus and a line focus,

wherein the piezoelectric ultrasound therapy element is configured to increase the temperature of the tissue in the region of interest to greater than 60° C.,

wherein the piezoelectric ultrasound therapy element is a single element that delivers ultrasound energy at a frequency of between 2 MHz to 25 MHz.

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3. The ultrasound probe of claim 1, further comprising a piezoelectric ultrasound imaging element co-housed with the piezoelectric ultrasound therapy element.

4. The ultrasound probe of claim 1, wherein the ultrasound probe is reusable, wherein the housing is configured for connection to a control system,

wherein the control system comprises a microprocessor and a communication device,
wherein the ultrasound transducer is electrically connected to the control system via a cable.

5. The ultrasound probe of claim 1, further comprising an EEPROM to store and record probe identification and usage history,

wherein the ultrasound therapy energy is configured to deliver an energy level for causing at least one of shrinking collagen and denaturing the tissue in the region of interest proximate a wrinkle,

wherein the piezoelectric ultrasound therapy element delivers the ultrasound therapy energy at a frequency of between 2 MHz to 25 MHz.

6. The ultrasound probe of claim 1, wherein the piezoelectric ultrasound therapy element is configured to connect to a control system and a power supply,

wherein the control system is connected to the motion mechanism, the piezoelectric ultrasound therapy element, and a power supply,

wherein the power supply is connected to the control system,

wherein the control system comprises a spatial control and a temporal control,

wherein the spatial control and the temporal control are configured for controlling the delivery of energy at a temperature sufficient to cause denaturation of at least the portion of the tissue at the one or more depths under the skin surface, wherein the spatial control and the temporal control are configured for controlling the delivery of energy at a frequency of between 2 MHz to 25 MHz.

7. An ultrasound probe for treatment of skin laxity, the ultrasound probe comprising:

an ultrasound transducer within a housing, the ultrasound transducer being configured for delivery of an ultrasound therapy energy at a temperature sufficient to heat at least a portion of a tissue at a one or more depths under a skin surface,

wherein the tissue comprises any one or more of the group consisting of: an epidermal tissue, a superficial dermal tissue, a mid-dermal tissue, a deep dermal tissue, a muscle tissue, and an adipose tissue;

wherein the ultrasound transducer comprises a single active piezoelectric ultrasound therapy element,

wherein the single active piezoelectric ultrasound therapy element with a mechanical focus configured to provide a thermal focus in the tissue at the one or more depths below a skin surface without a lens,

wherein the piezoelectric ultrasound therapy element is configured for delivery of the ultrasound therapy energy at the temperature sufficient to heat the at least a portion of the tissue at the one or more depths under the skin surface, wherein the ultrasound transducer forms a plurality of thermal lesions at the one or more depths for reducing the appearance of skin laxity.

8. The ultrasound probe of claim 7, further comprising a storage system comprising probe identification and probe usage history, wherein the region of interest comprises the tissue, wherein the skin surface comprises a wrinkle, and wherein the plurality of thermal lesions tightens the tissue.

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9. The ultrasound probe of claim 7, further comprising a piezoelectric ultrasound imaging element co-housed with the piezoelectric ultrasound therapy element, wherein the piezoelectric ultrasound therapy element delivers the ultrasound therapy energy at a frequency of between 2 MHz to 50 MHz.

10. The ultrasound probe of claim 7, wherein the ultrasound probe is reusable, wherein the piezoelectric ultrasound therapy element is configured for communication with a control system, wherein the ultrasound transducer is connected to the control system via a cable, and wherein the control system comprises:

a communication device;

a processor, software, an input device, and a power supply.

11. The ultrasound probe of claim 7,

wherein the piezoelectric ultrasound therapy element is a single element that delivers the ultrasound therapy energy at a frequency of between 2 MHz to 25 MHz,

wherein the piezoelectric ultrasound therapy element is configured to increase the temperature of the tissue in the region of interest to greater than 60° C.,

wherein the ultrasound probe is disposable,

and wherein the ultrasound probe comprises a storage system for transducer usage history and calibration.

12. An ultrasound probe for treatment of skin laxity, the ultrasound probe comprising:

a housing and an ultrasound transducer, wherein the ultrasound transducer is inside the housing,

wherein the ultrasound transducer comprises a piezoelectric ultrasound therapy element,

wherein the piezoelectric ultrasound therapy element is configured to provide a thermal lesion via a mechanical focus without a lens in a tissue at at least one depth below a skin surface,

wherein the at least one depth is up to 5 mm below the skin surface,

wherein the tissue comprises any of the group consisting of: an epidermal tissue, a superficial dermal tissue, a mid-dermal tissue, a deep dermal tissue, an adipose tissue, and a muscle tissue,

wherein the piezoelectric ultrasound therapy element is configured for delivery of the ultrasound therapy energy at a temperature sufficient to denature at least a portion of the tissue in the region of interest at the at least one depth under the skin surface,

wherein the piezoelectric ultrasound therapy element forms a plurality of the thermal lesions at the at least one depth for tightening the tissue for reducing skin laxity.

13. The ultrasound probe of claim 12, further comprising a control system and a power supply;

wherein the ultrasound therapy element is in communication with the control system,

wherein the ultrasound transducer is connected to the control system via a cable,

wherein the skin surface comprises a wrinkle.

14. The ultrasound probe of claim 12, further comprising an acoustic coupler between the ultrasound transducer and the skin surface, wherein the piezoelectric ultrasound therapy element is a single element that delivers ultrasound energy at a frequency of between 2 MHz to 25 MHz.

15. The ultrasound probe of claim 12, wherein the ultrasound probe is disposable, wherein the piezoelectric ultrasound therapy element is configured to increase the temperature of the tissue in a region of interest to greater than 60° C.

16. The ultrasound probe of claim 12, further comprising a storage system and a piezoelectric ultrasound imaging element, wherein the storage system records probe usage history, and wherein the piezoelectric ultrasound imaging element is co-housed with the piezoelectric ultrasound therapy element in the housing. 5

17. The ultrasound probe of claim 12, further comprising a monitoring system, wherein the monitoring system is configured to monitor a treatment parameter, wherein the treatment parameter measured comprises a temperature of the tissue below the skin surface. 10

18. The ultrasound probe of claim 12, further comprising a motion mechanism configured to operate with an encoder, wherein the motion mechanism is configured for movement of the piezoelectric ultrasound therapy element to form a plurality of thermal lesions at the at least one depth in the region of interest. 15

19. The ultrasound probe of claim 12, further comprising a motion mechanism configured to operate with an encoder, wherein the motion mechanism is configured for any one of the group consisting of linear, rotational, and variable movement of the piezoelectric ultrasound therapy element. 20

20. The ultrasound probe of claim 12, further comprising a motion mechanism configured to operate with an encoder for monitoring a position of the ultrasound therapy element, wherein the piezoelectric ultrasound therapy element is a single element that delivers the ultrasound therapy energy at a frequency of between 2 MHz to 25 MHz, wherein the piezoelectric ultrasound therapy element is configured to deliver the ultrasound therapy energy at the at least one depth below the skin surface. 25 30

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专利名称(译)	超声探头治疗皮肤松弛		
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外部链接	Espacenet		

摘要(译)

提供了一种用于皮肤松弛的超声治疗的探针。系统和方法可以包括感兴趣区域的超声成像，用于治疗区域的定位，以深度和模式递送超声能量以实现期望的治疗效果，和/或监测治疗区域以评估结果和/或提供反馈。在一个实施例中，治疗系统和方法可以被配置用于产生亚毫米和更大的热消融区域的阵列，以治疗组织的表皮，表皮，真皮或深层真皮组件。

