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- (54) **MONITORING AND NOISE MASKING OF THERMAL THERAPY**
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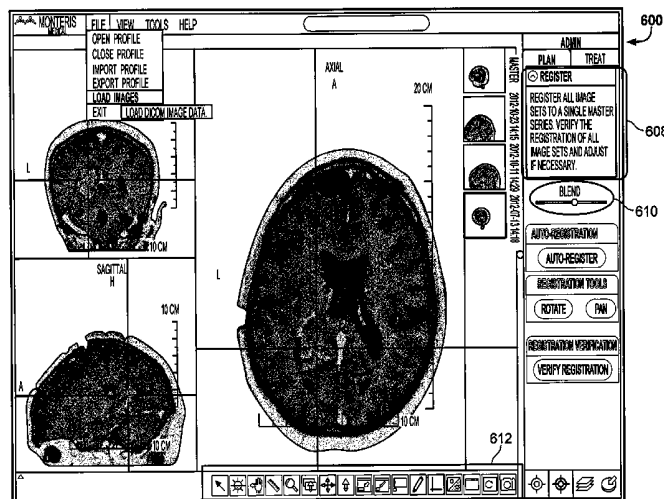
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(57) **ABSTRACT**

Image-guided therapy of a tissue can utilize magnetic resonance imaging (MRI) or another medical imaging device to guide an instrument within the tissue. A workstation can actuate movement of the instrument, and can actuate energy emission and/or cooling of the instrument to effect treatment to the tissue. The instrument can be an MRI compatible laser probe that provides thermal therapy to, e.g., a tissue in a brain of a patient. By tracking a probe position within tissue through feedback, multiple data slices provided around the probe position can be processed to monitor treatment and view thermal data. The operator selects treatment area reference points with the assistance of noise masking.

20 Claims, 61 Drawing Sheets



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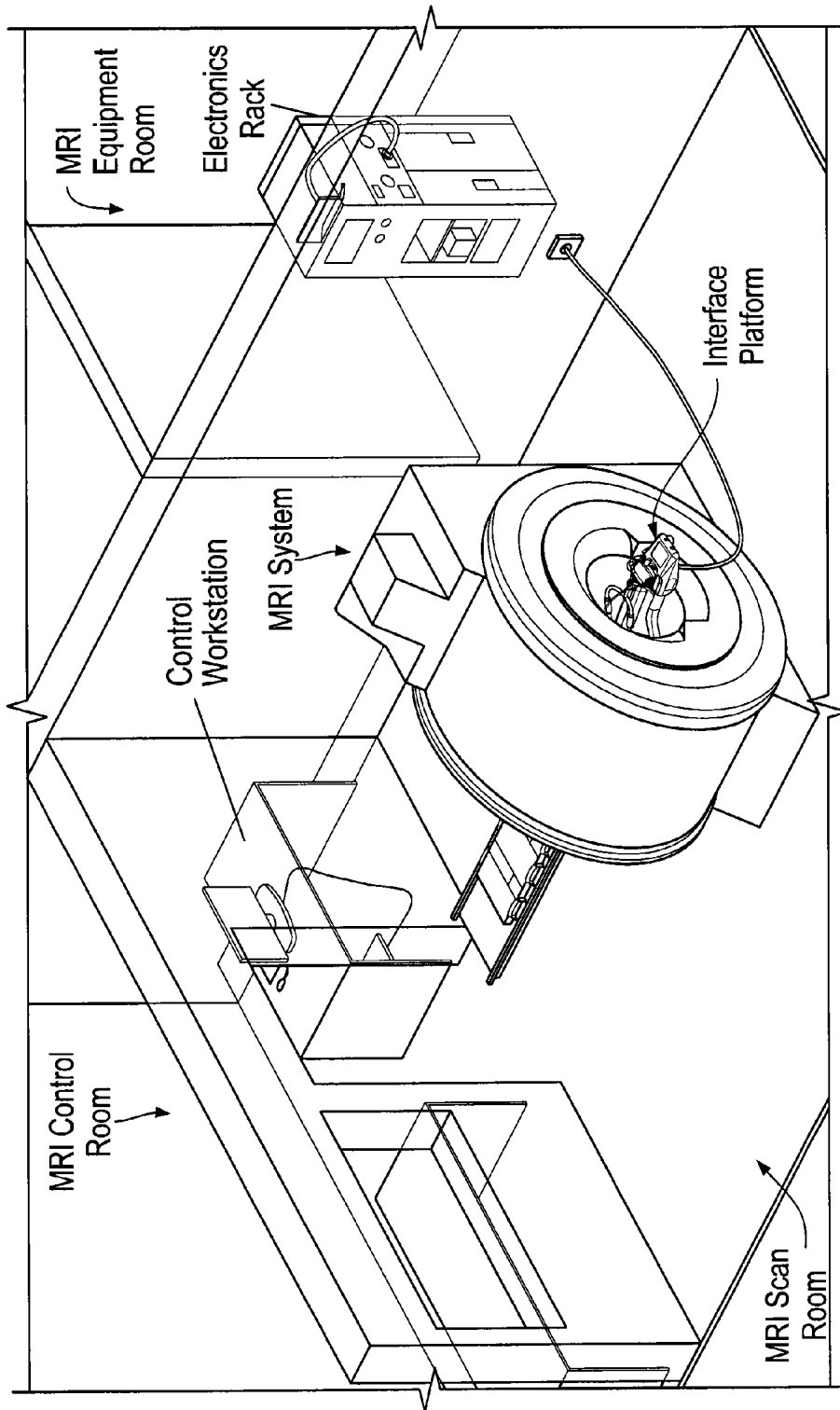
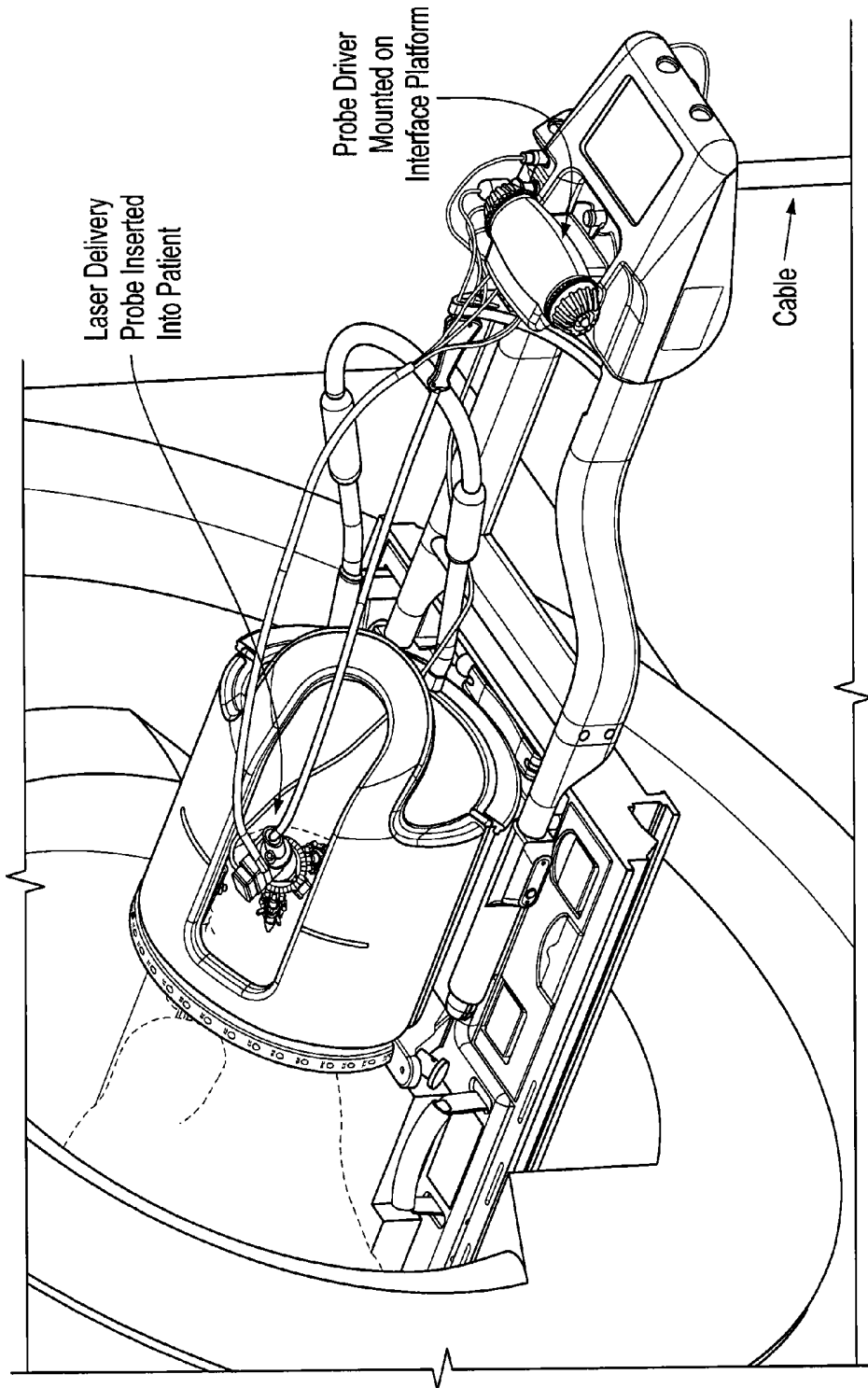


FIG. 1



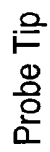
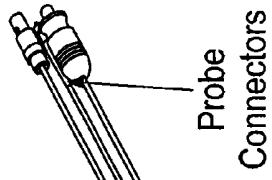


FIG. 3

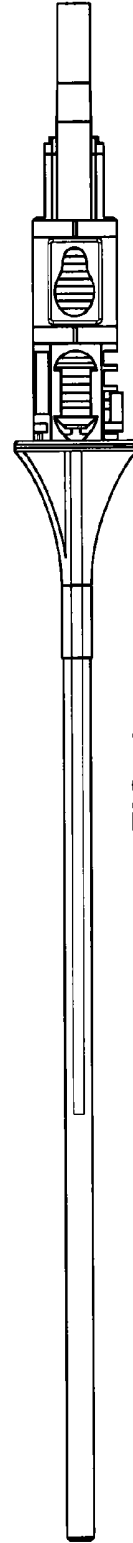


FIG. 4

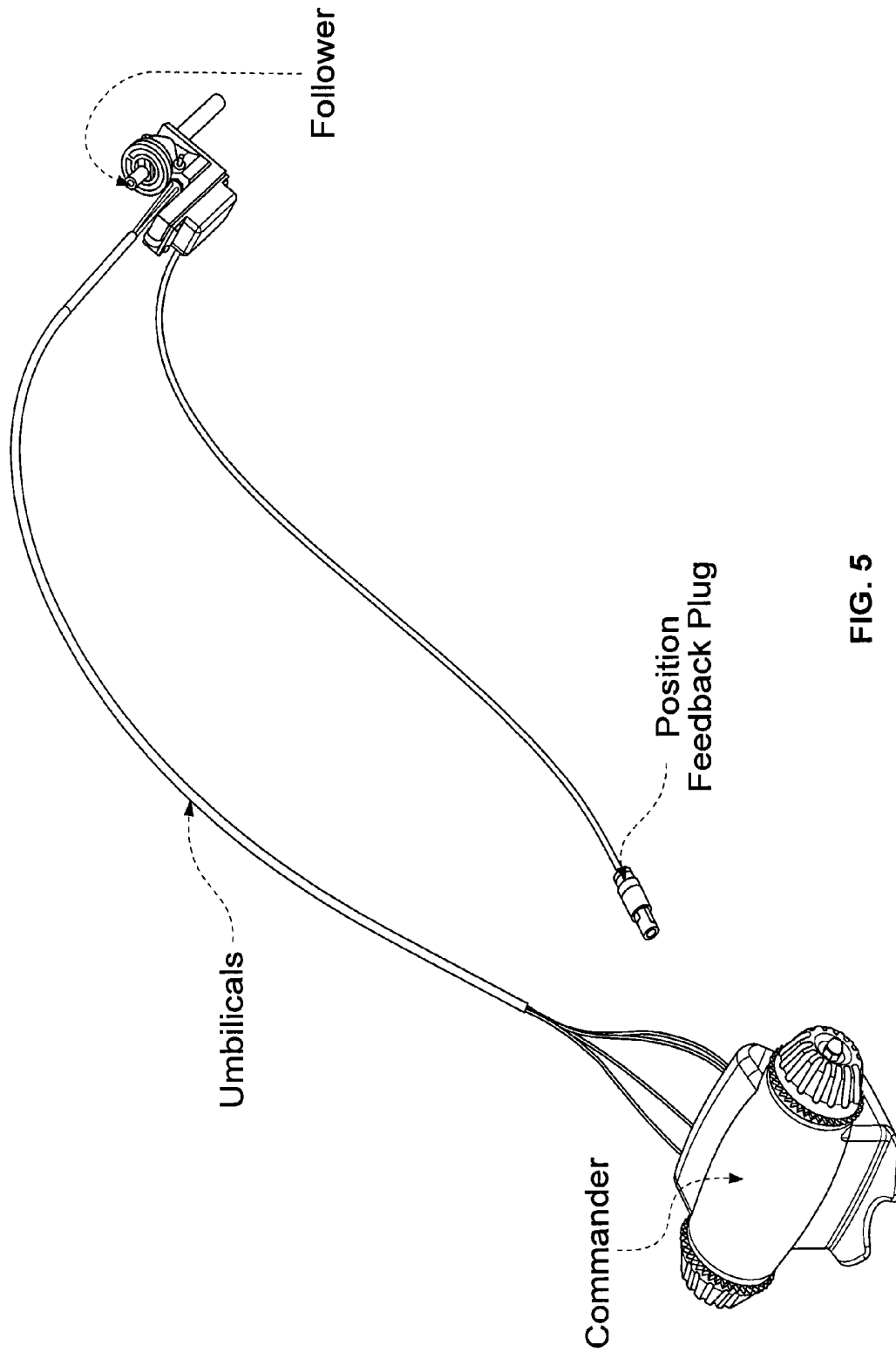


FIG. 5

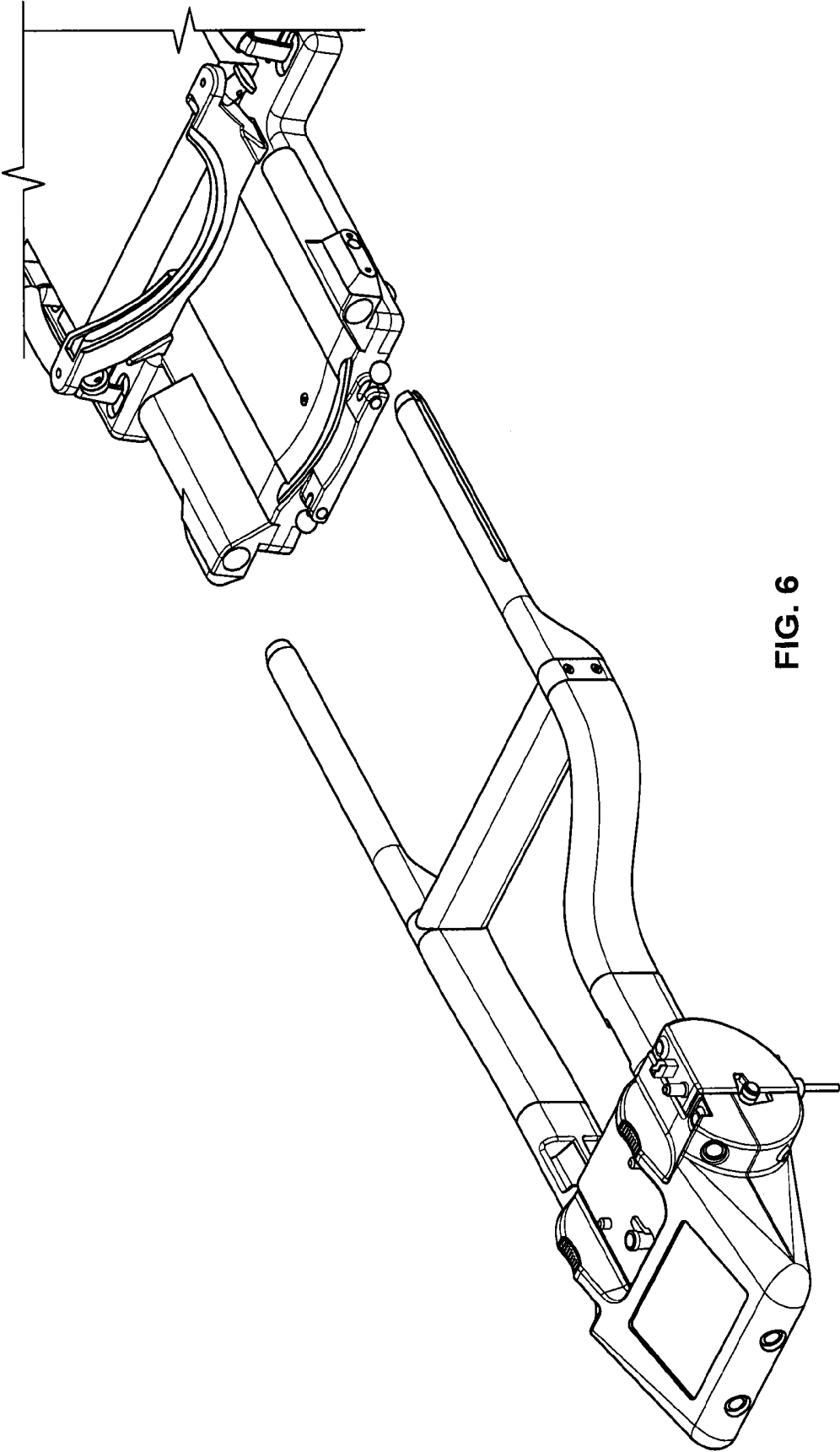


FIG. 6

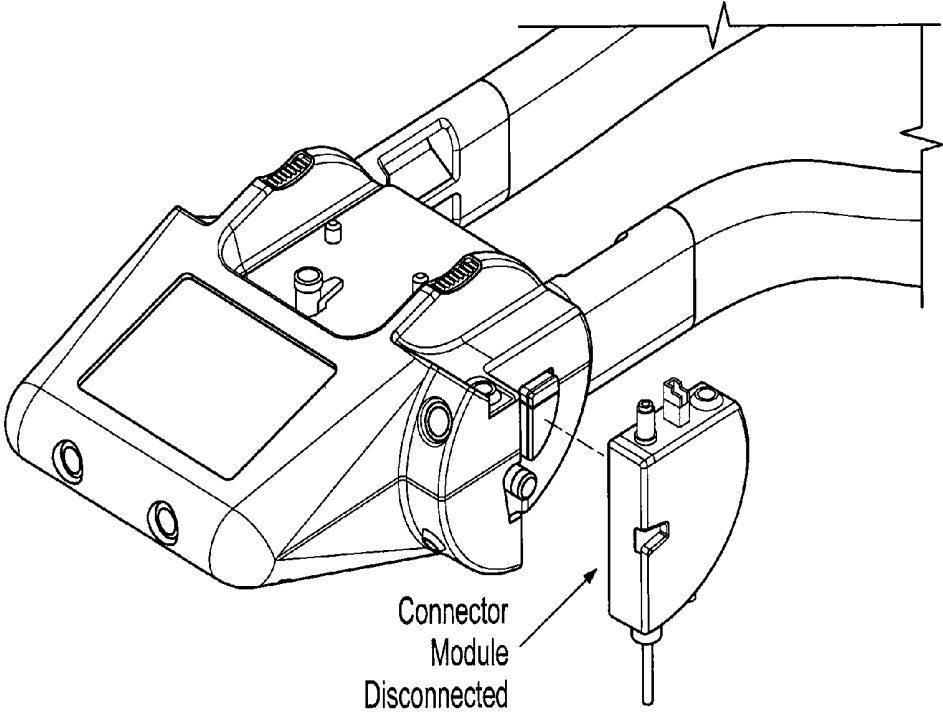


FIG. 7A

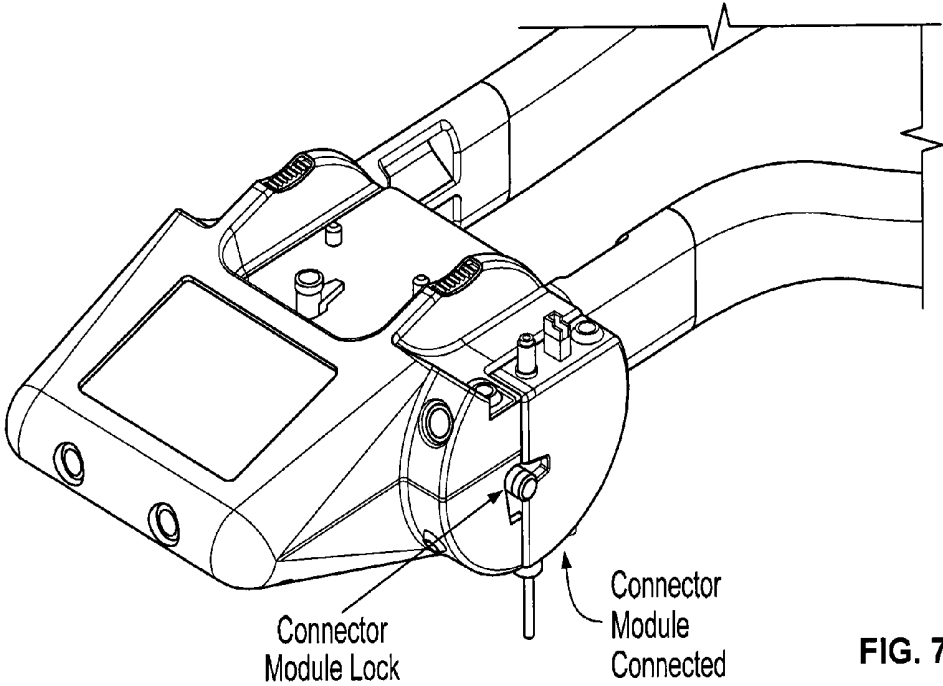


FIG. 7B

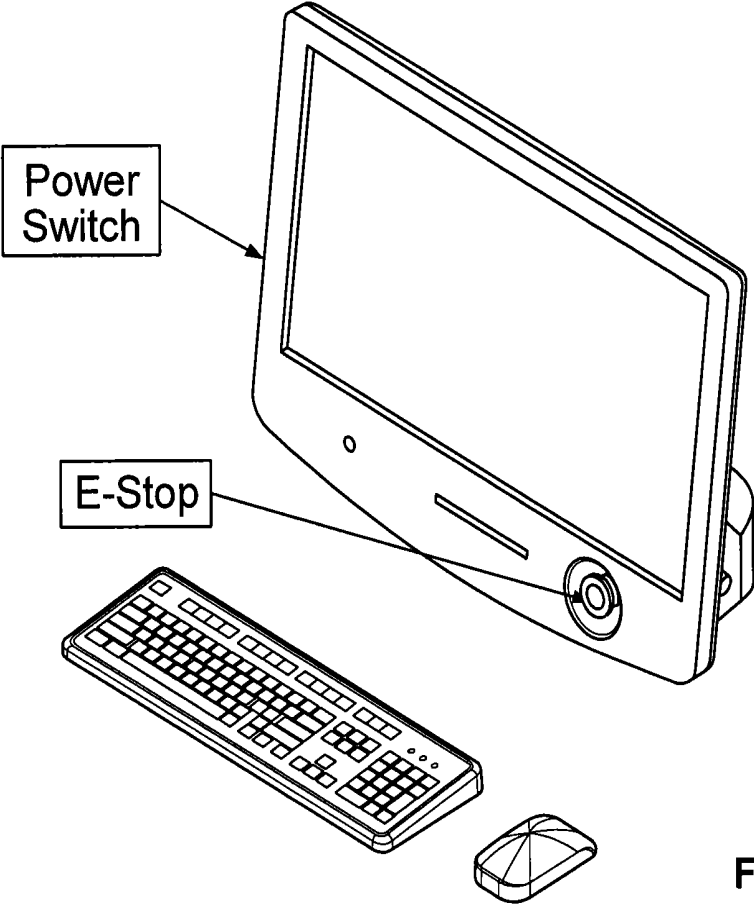


FIG. 8

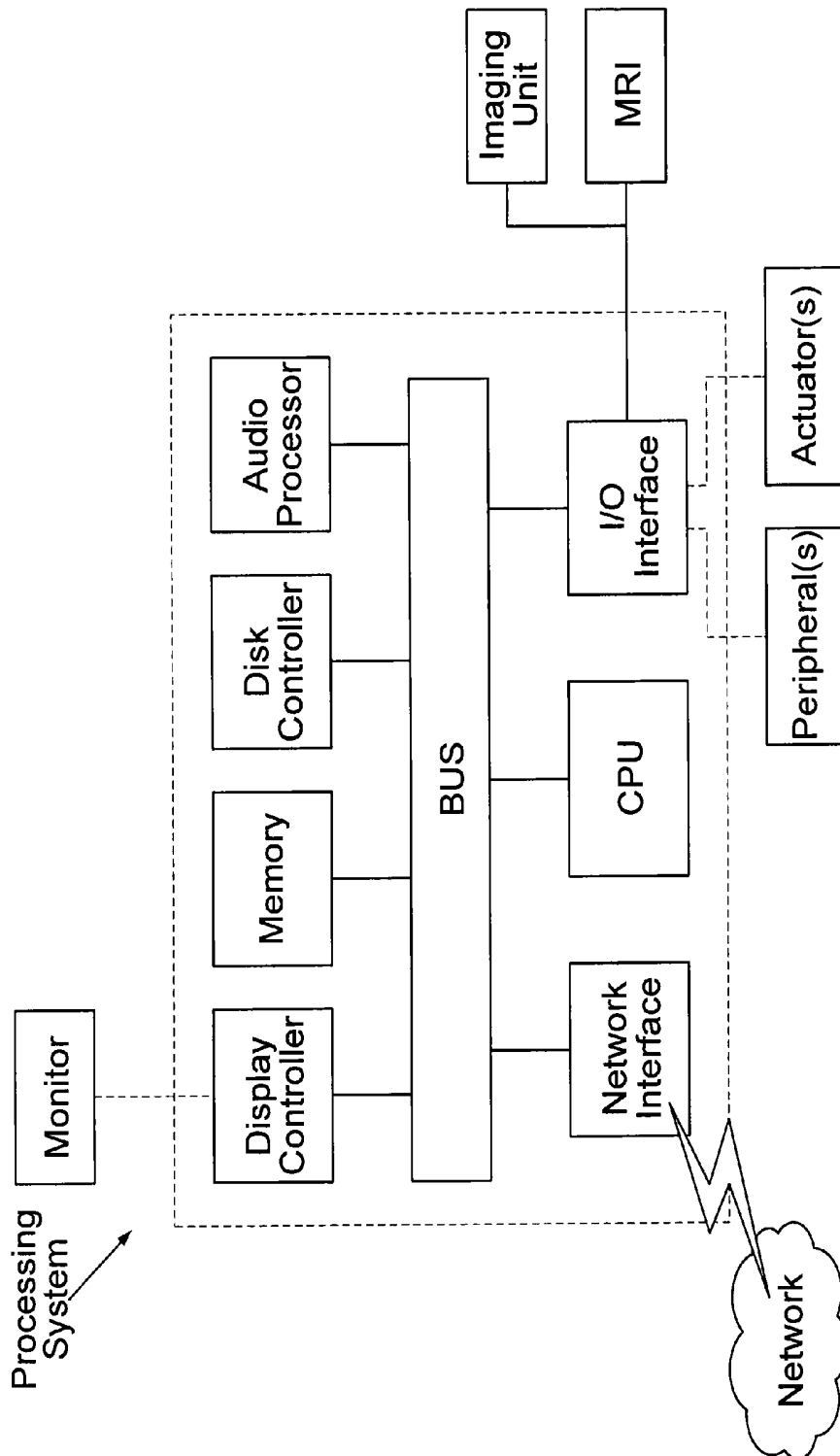


FIG. 9

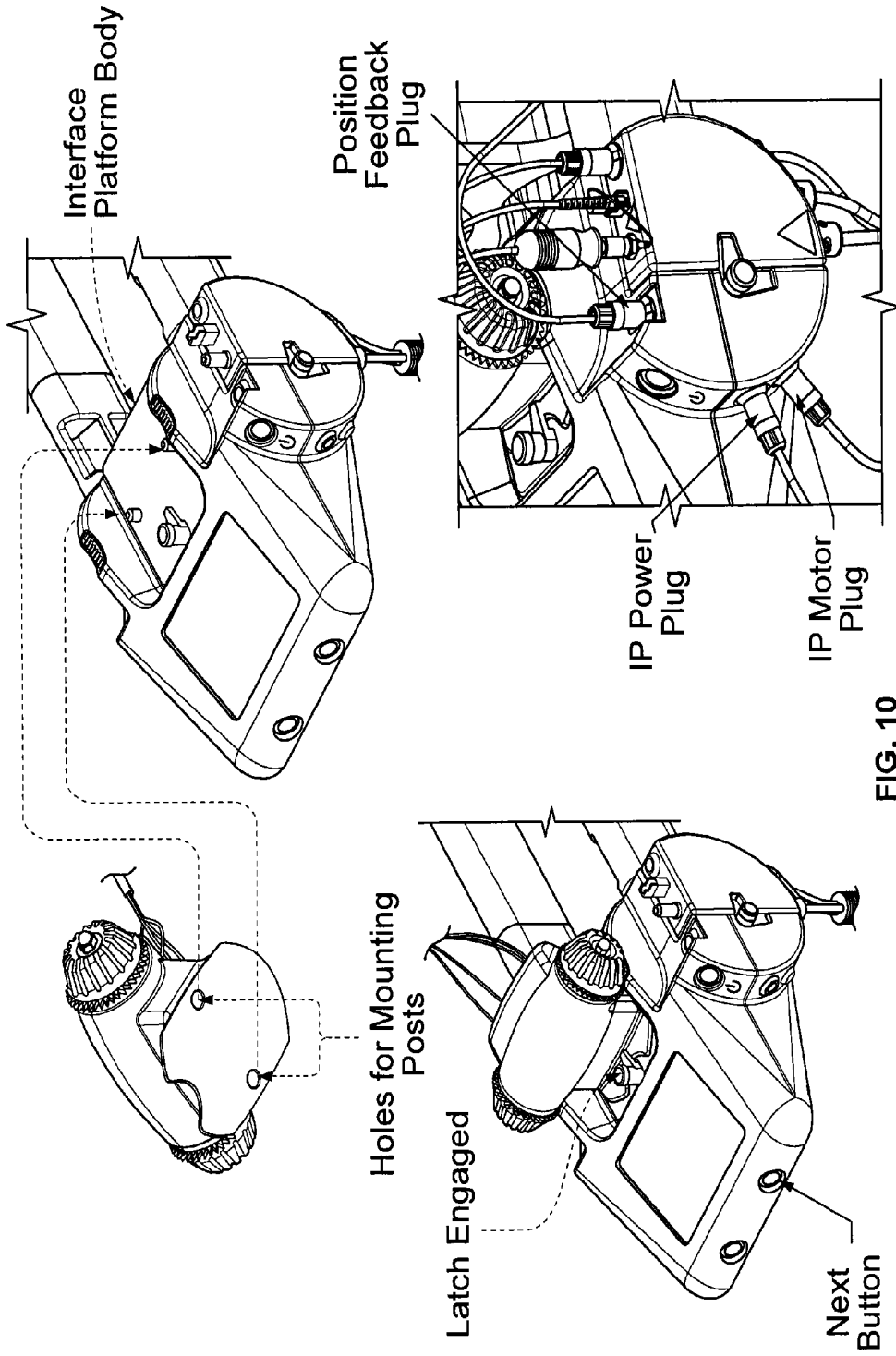
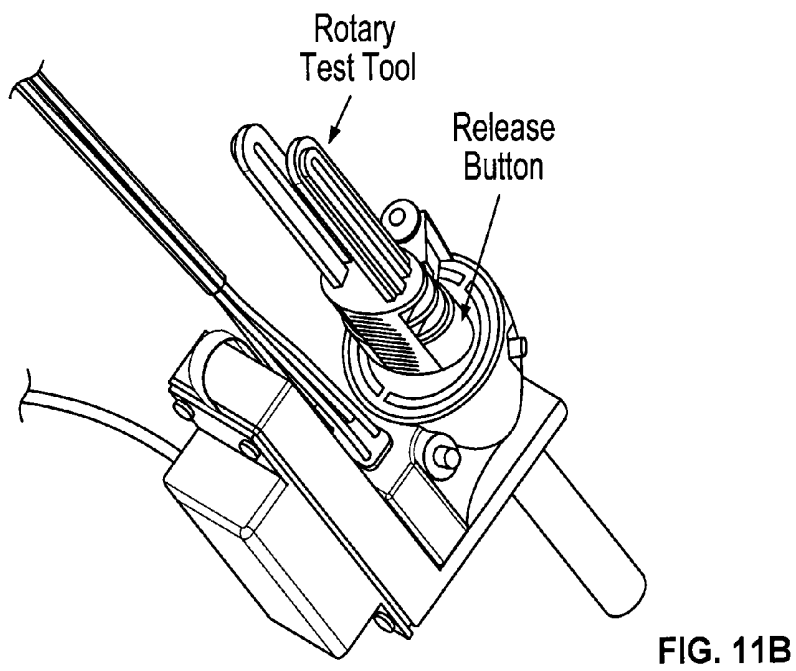
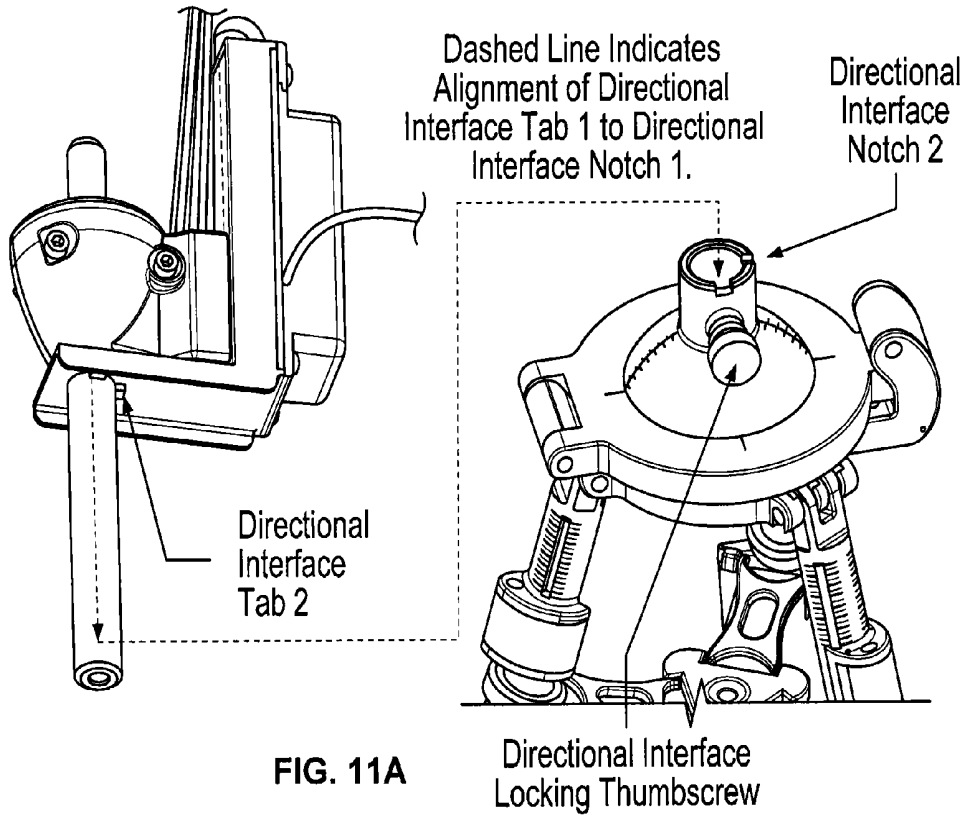


FIG. 10



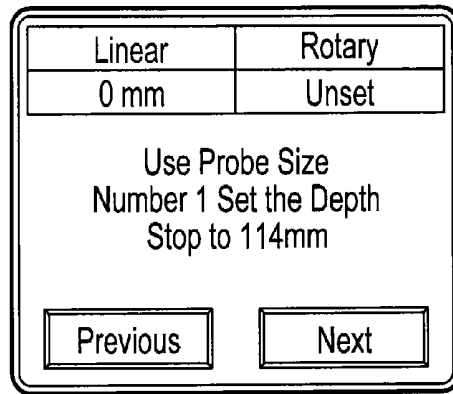


FIG. 12

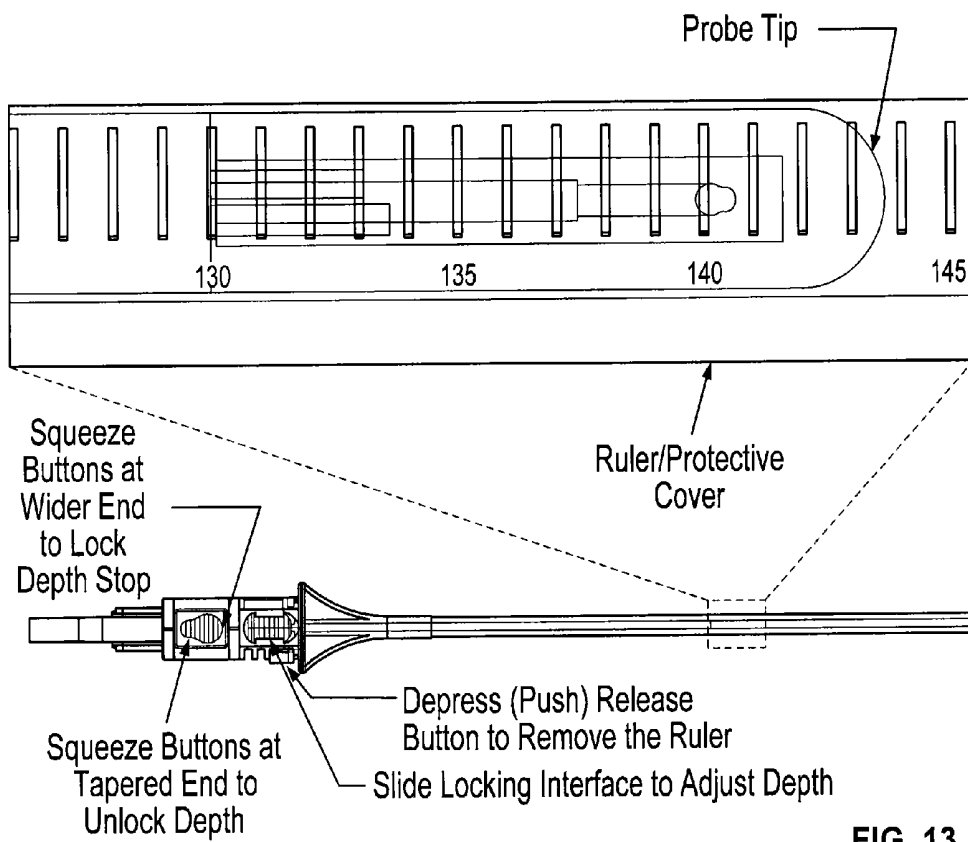


FIG. 13

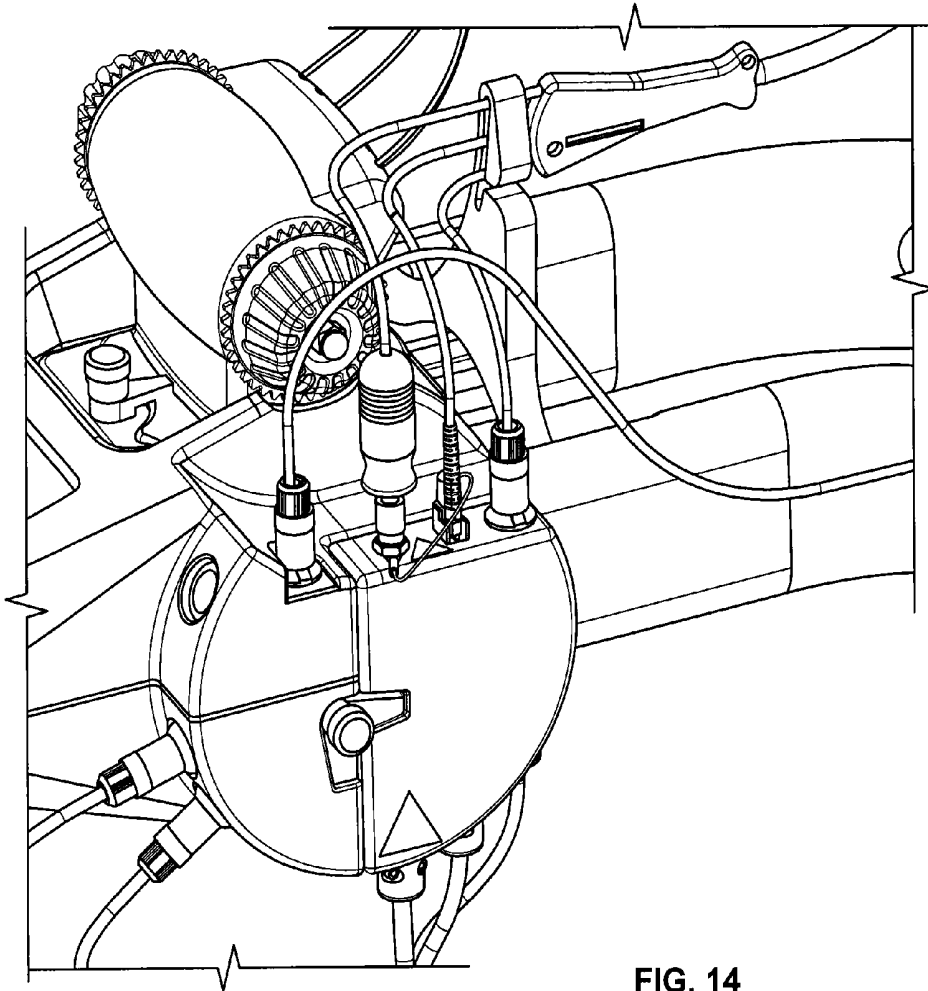


FIG. 14

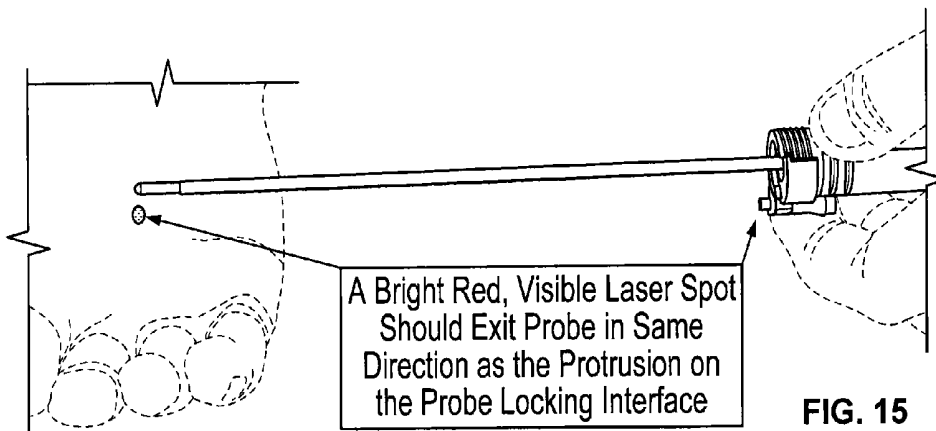


FIG. 15

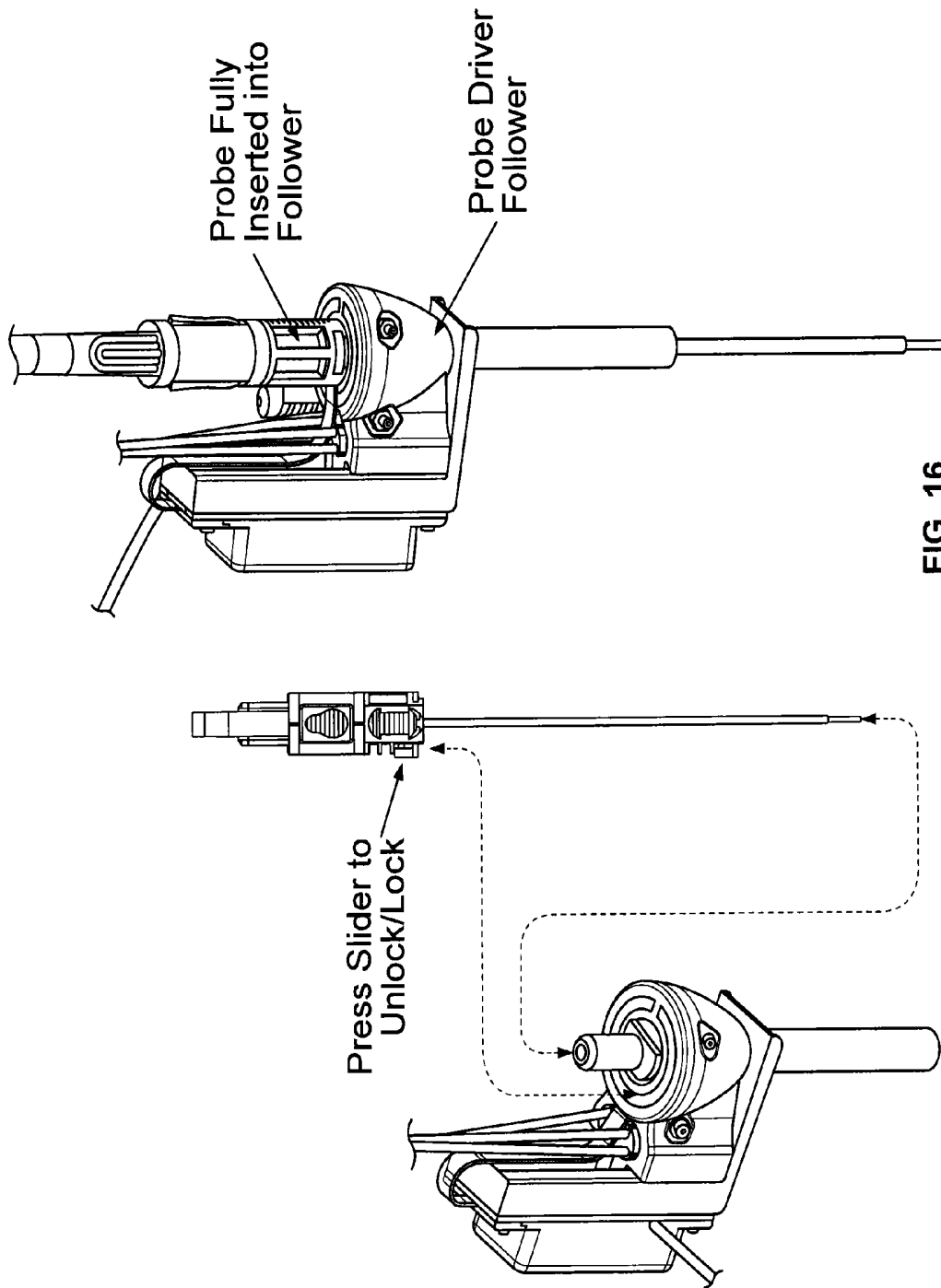


FIG. 16

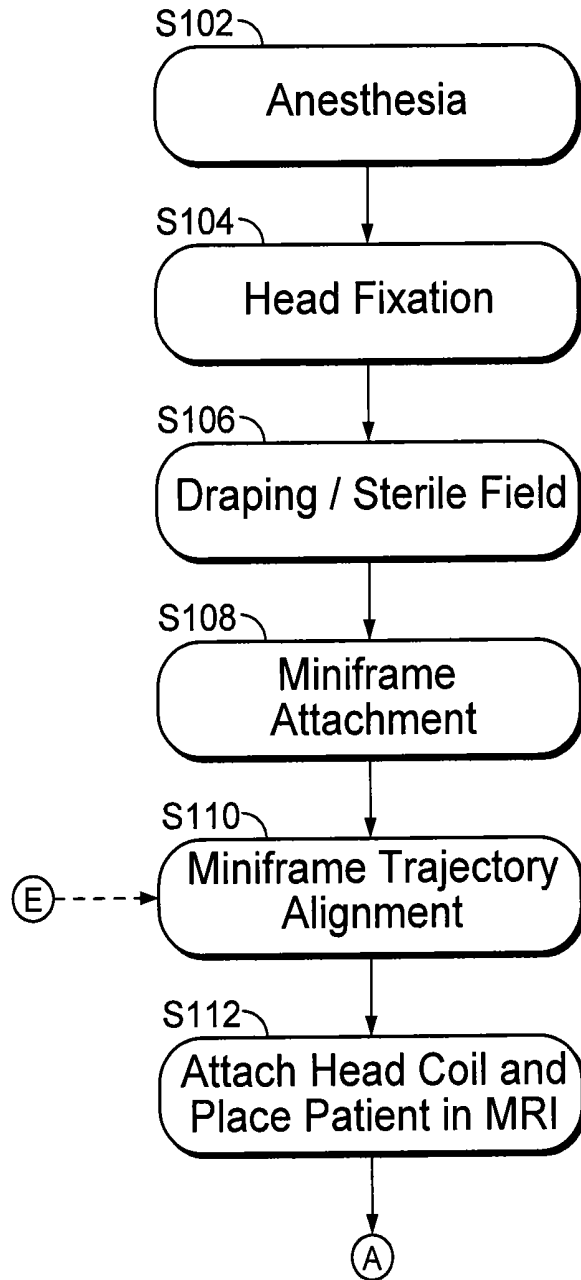


FIG. 17

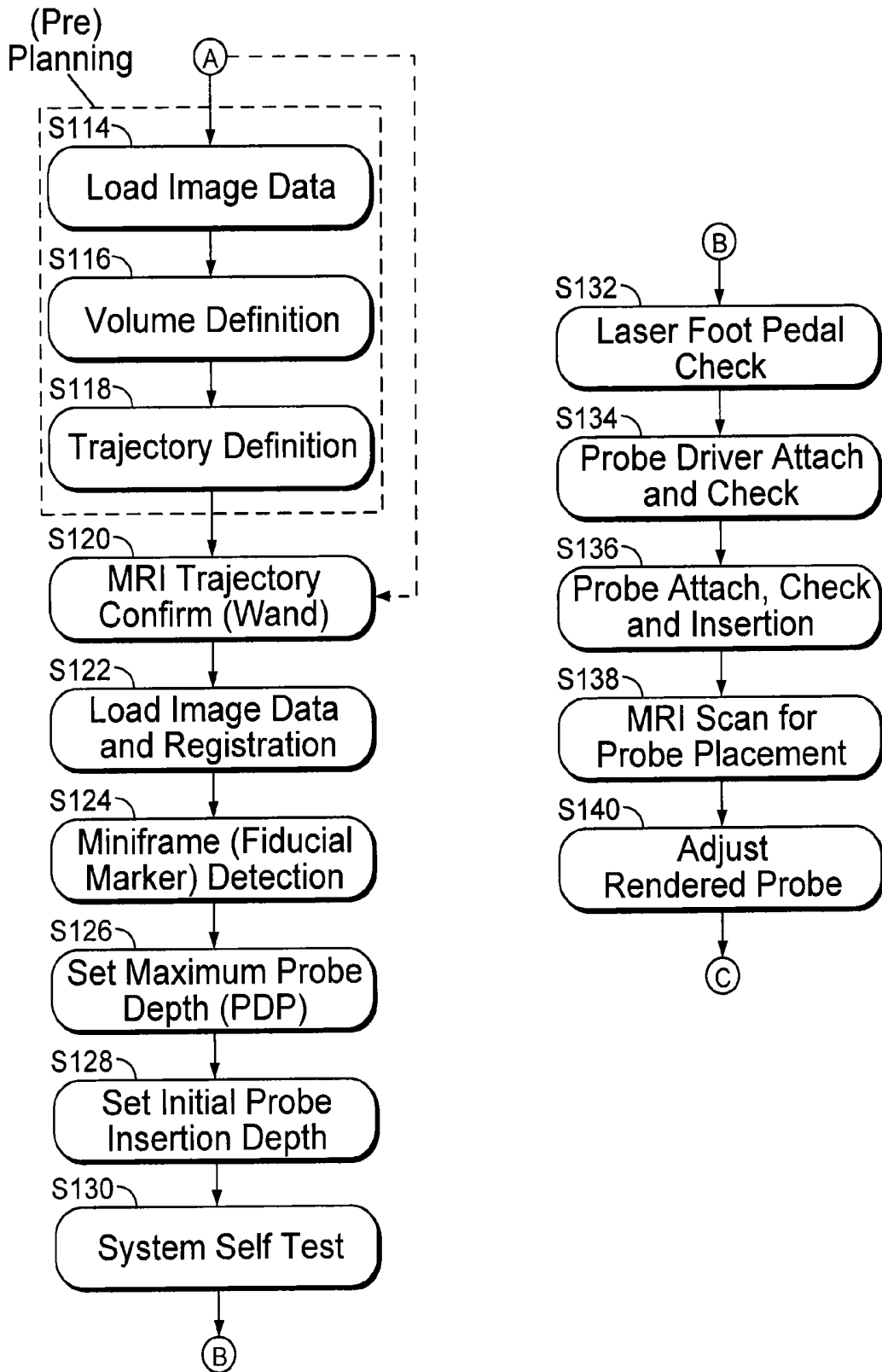


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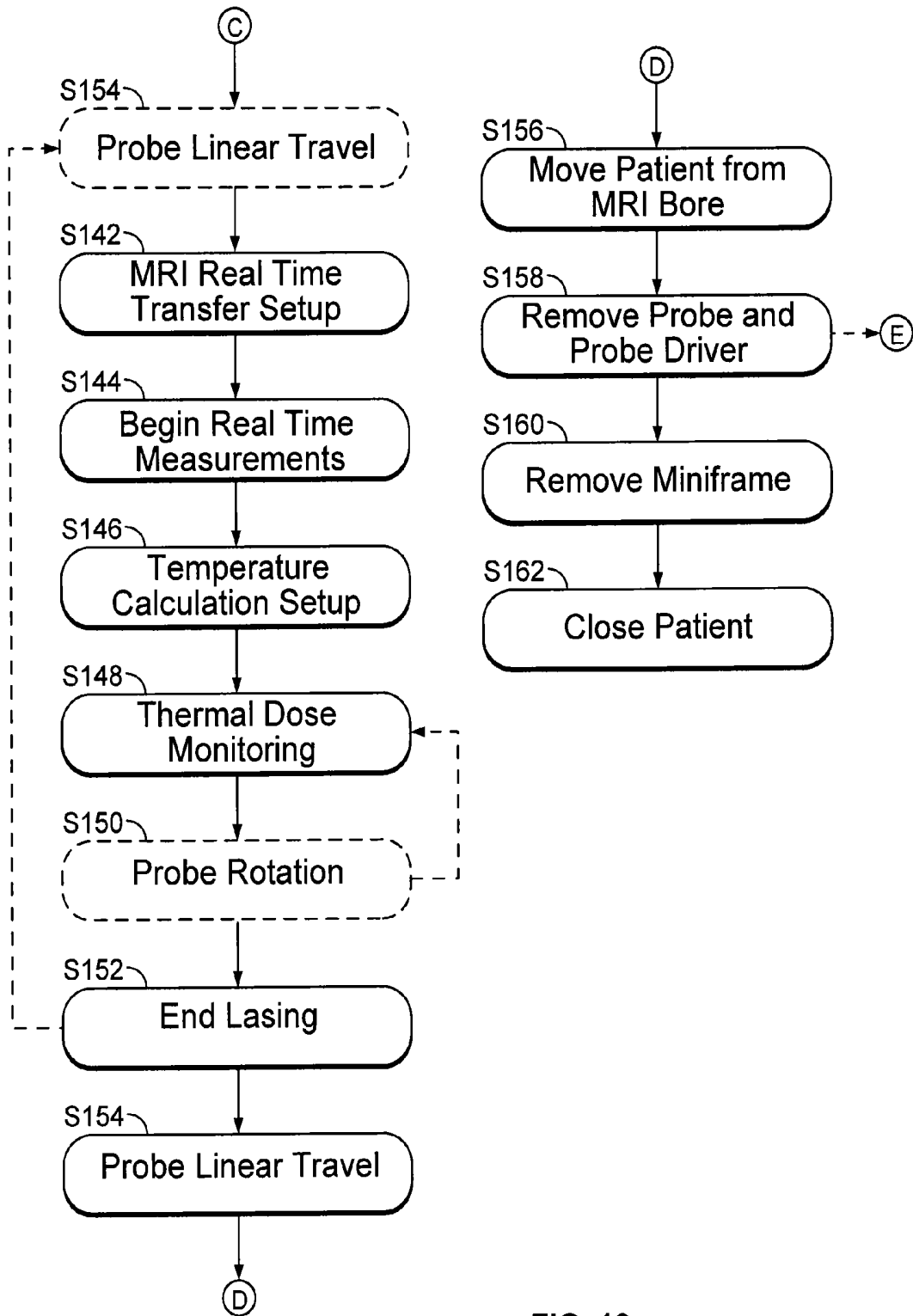


FIG. 19

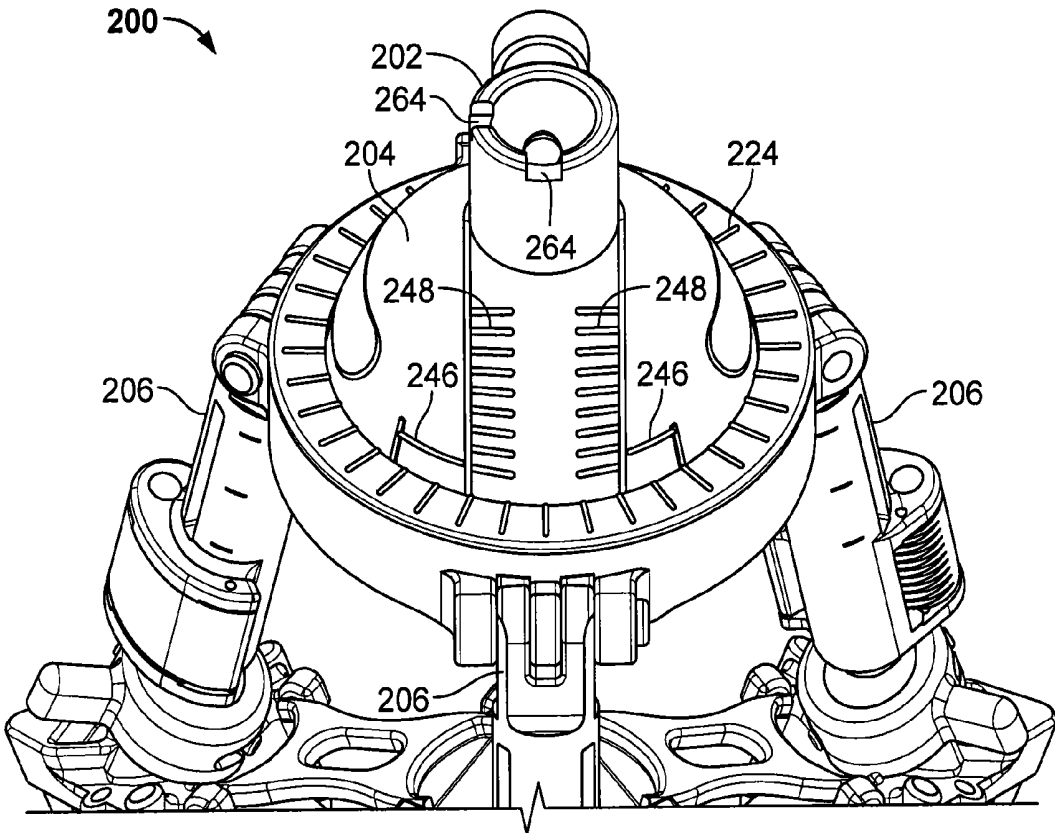


FIG. 20

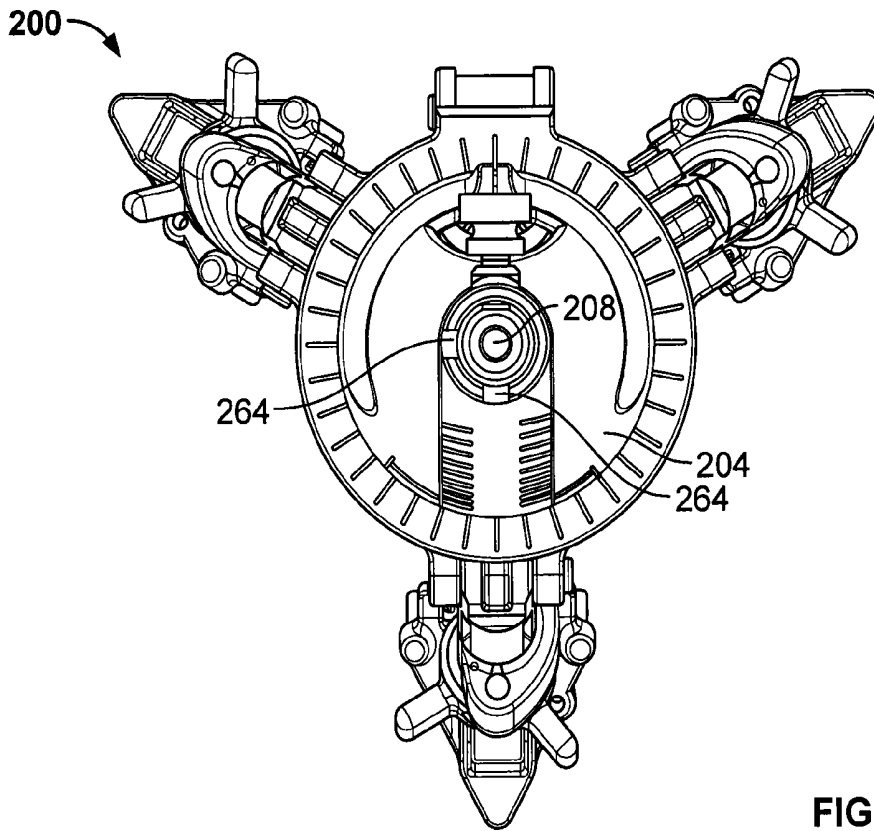


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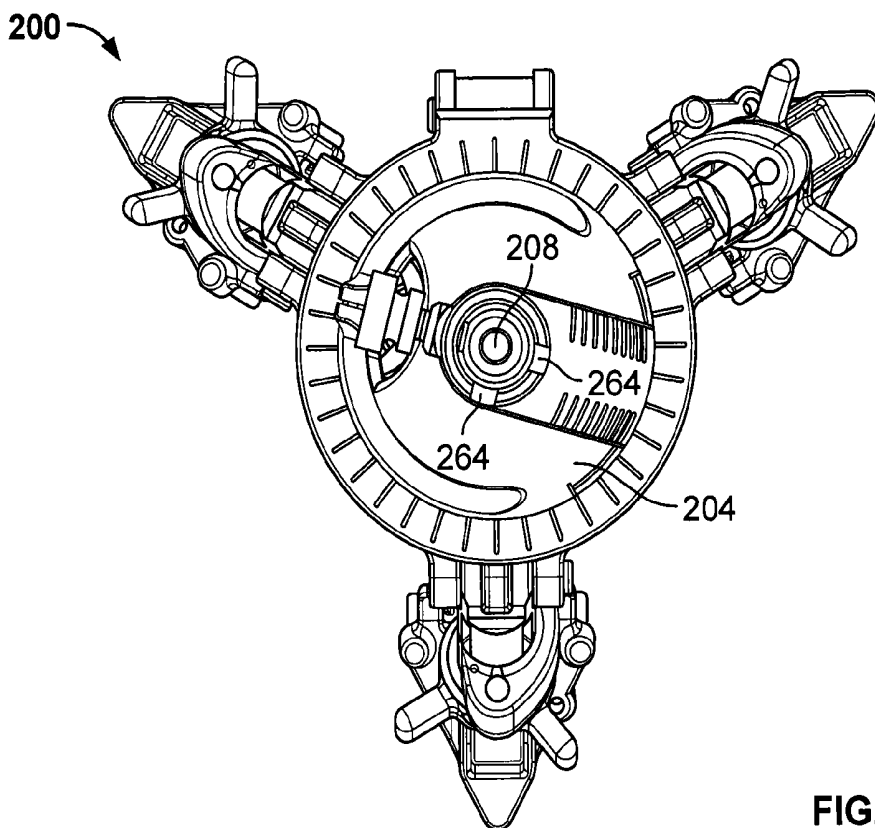


FIG. 22

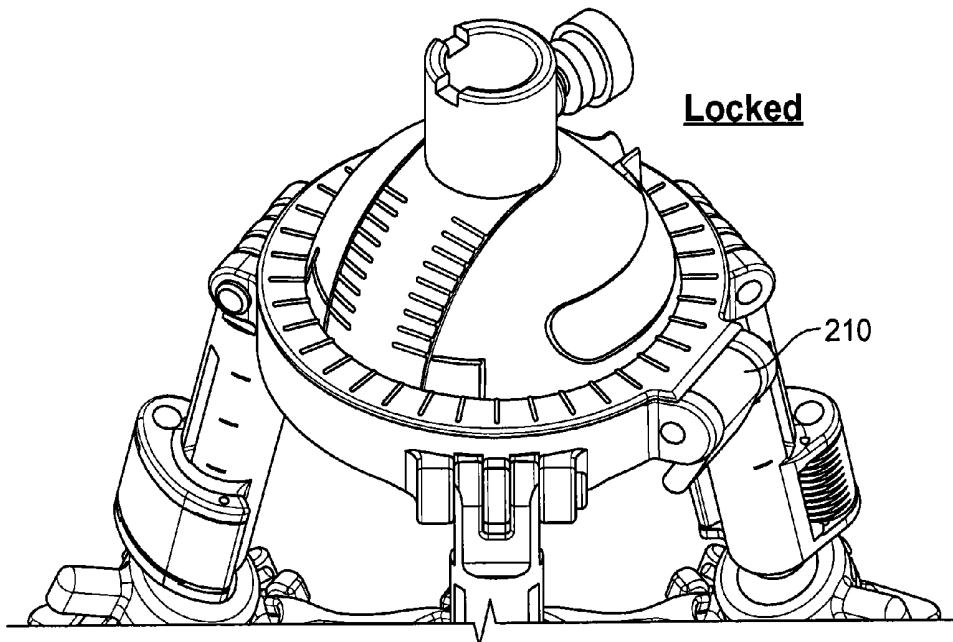


FIG. 23

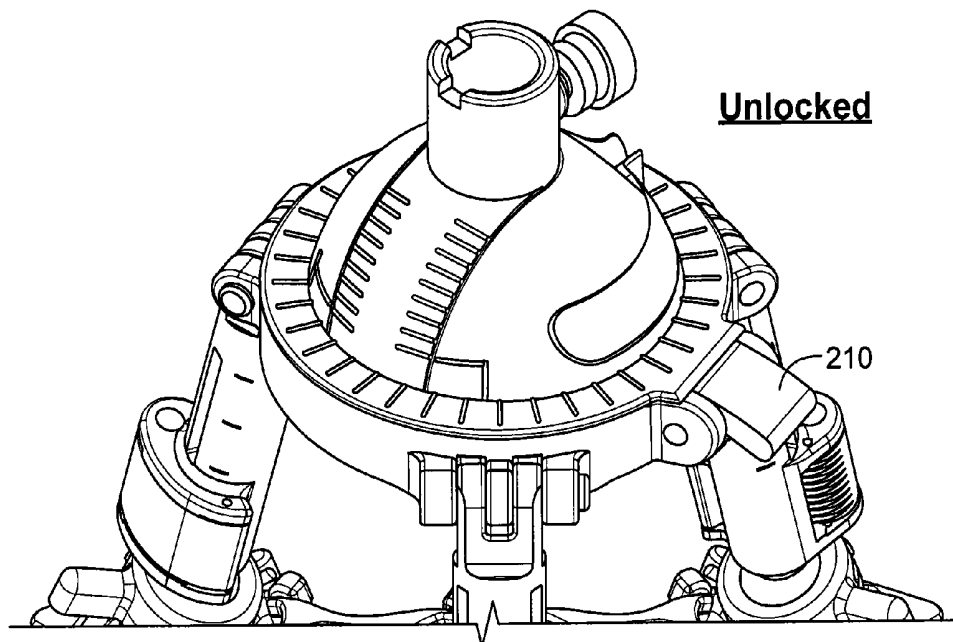


FIG. 24

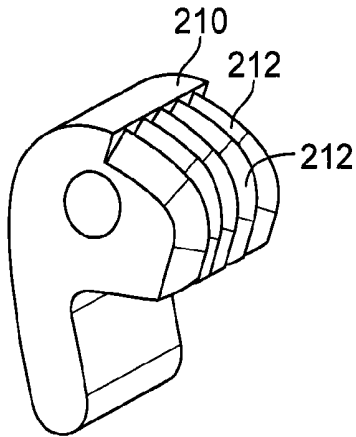


FIG. 25

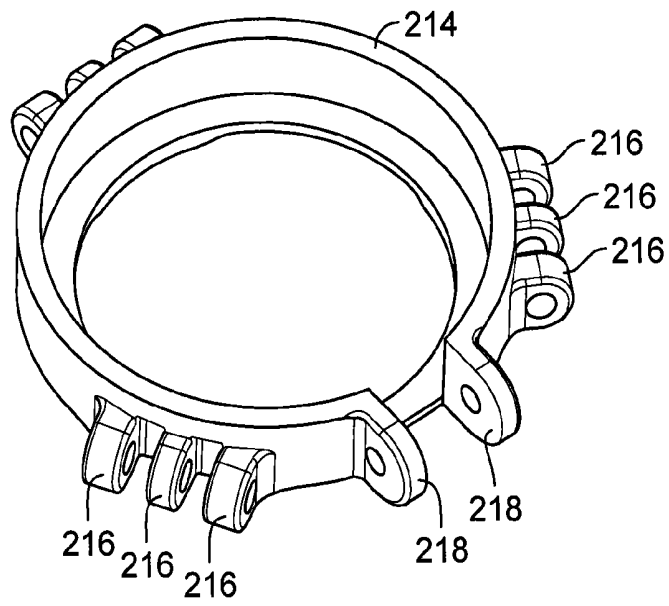


FIG. 26

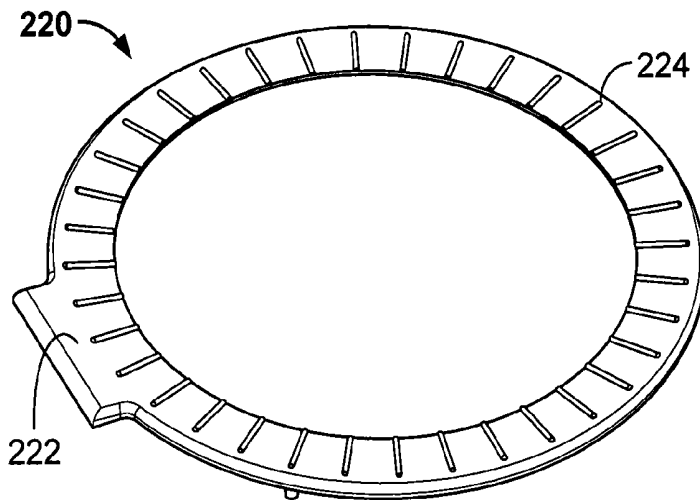


FIG. 27

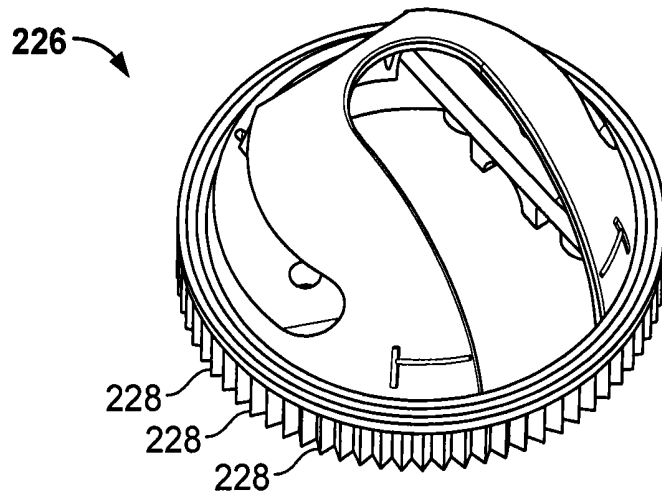


FIG. 28

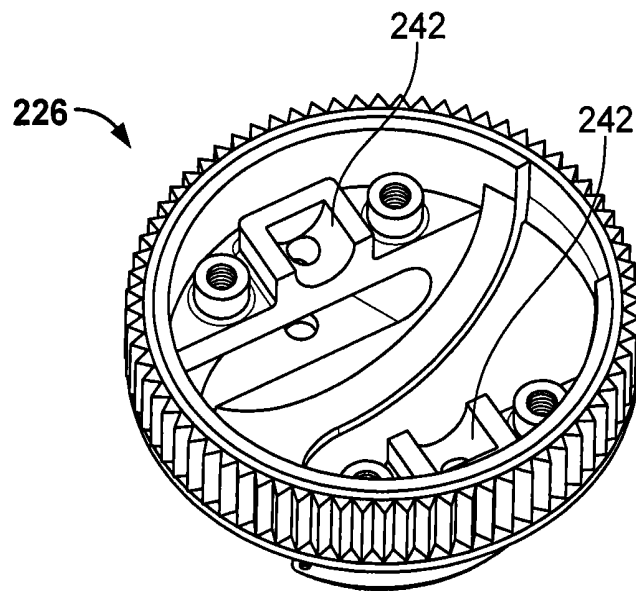
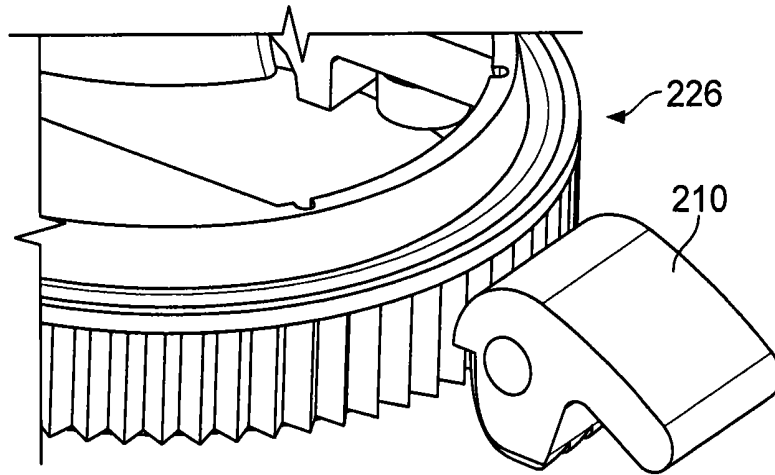
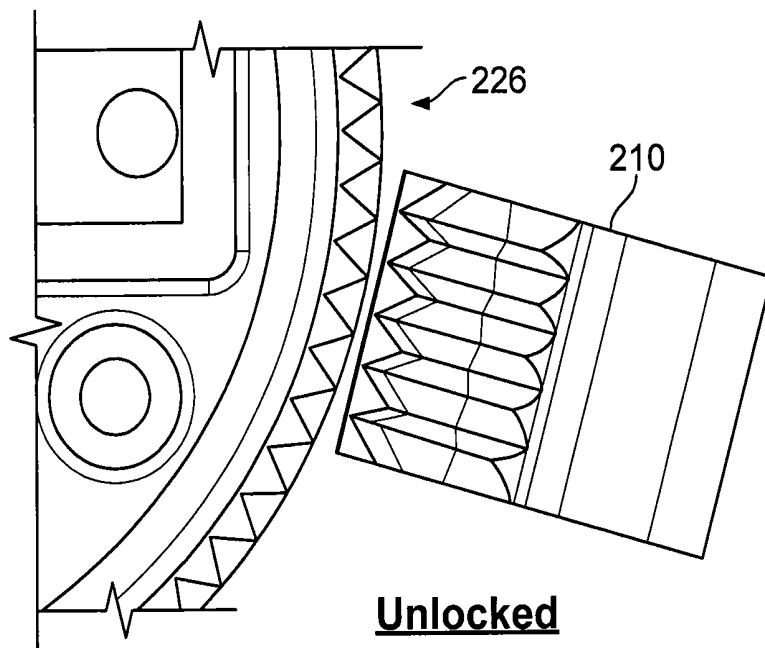


FIG. 29



Unlocked

FIG. 30



Unlocked

FIG. 31

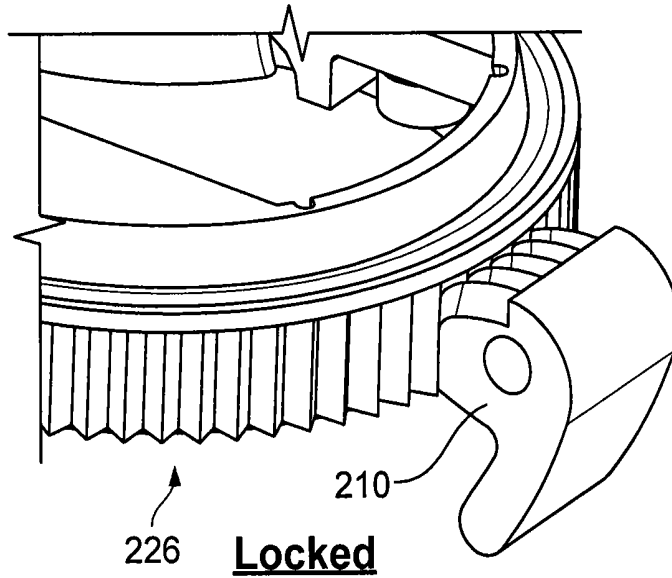


FIG. 32

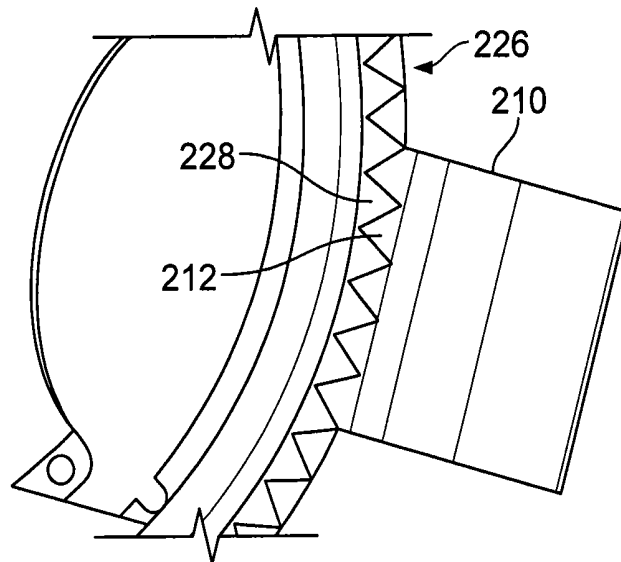


FIG. 33

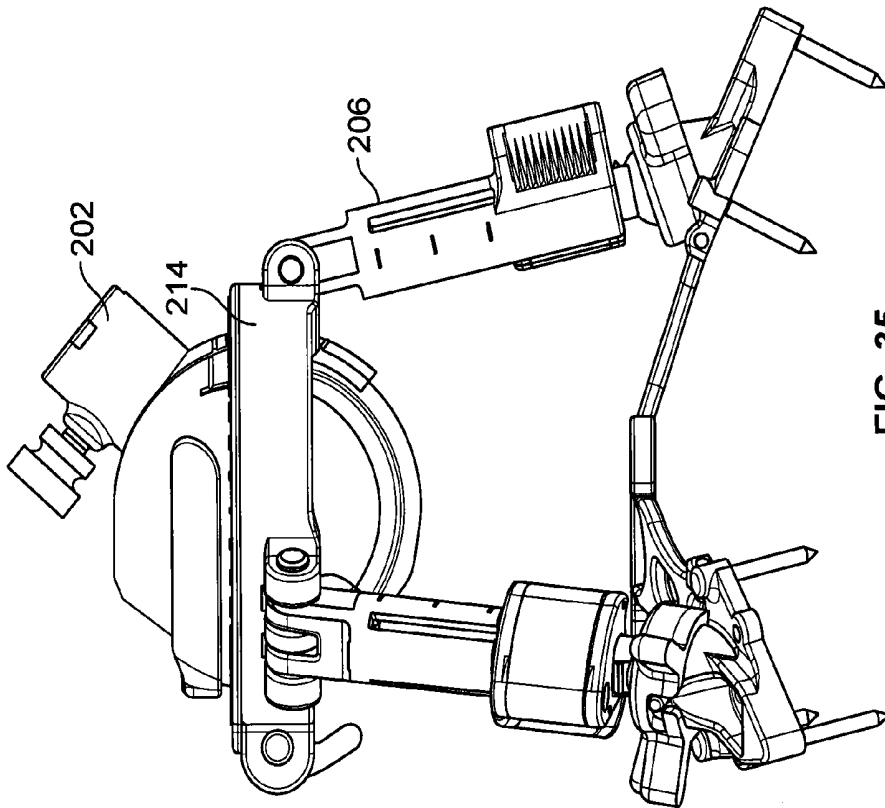


FIG. 35

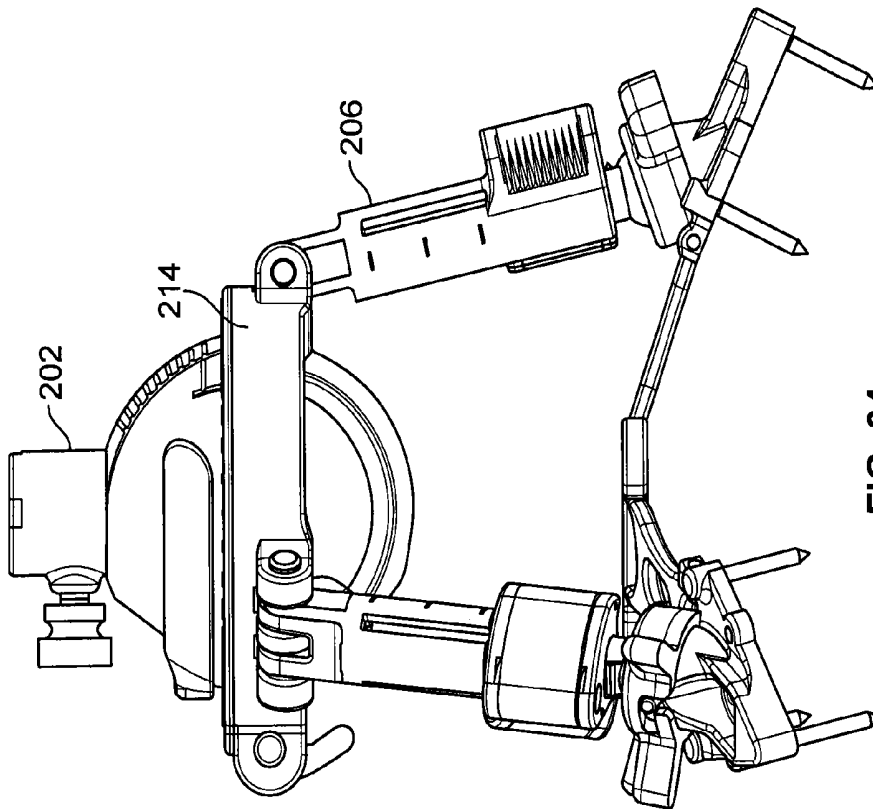


FIG. 34

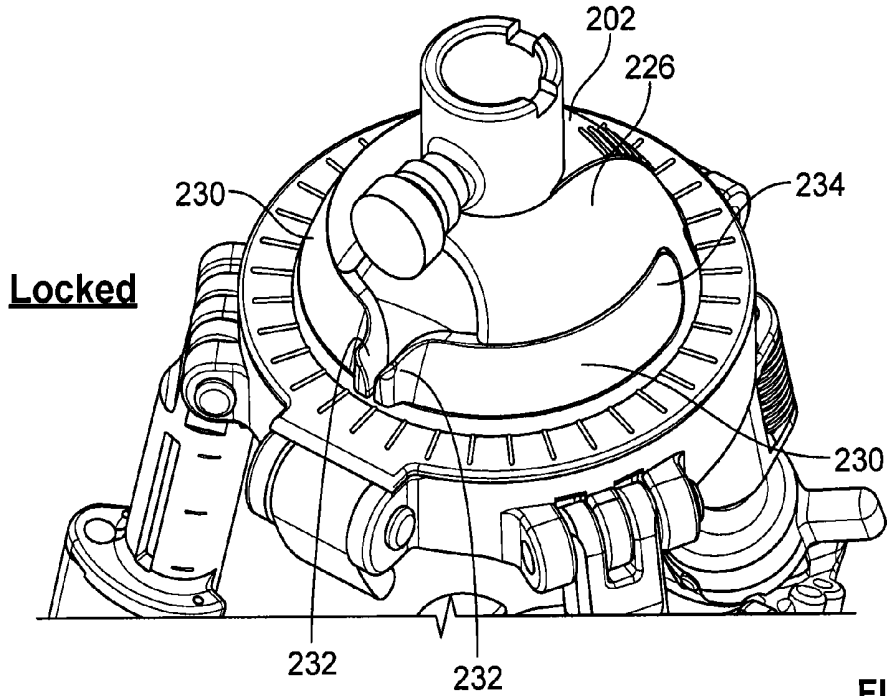


FIG. 36

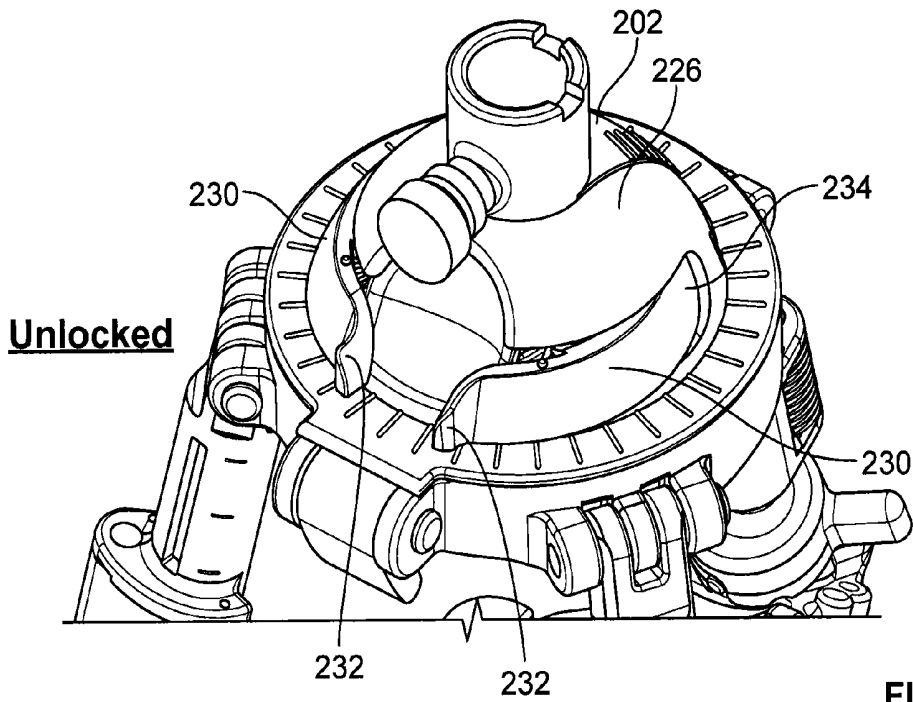


FIG. 37

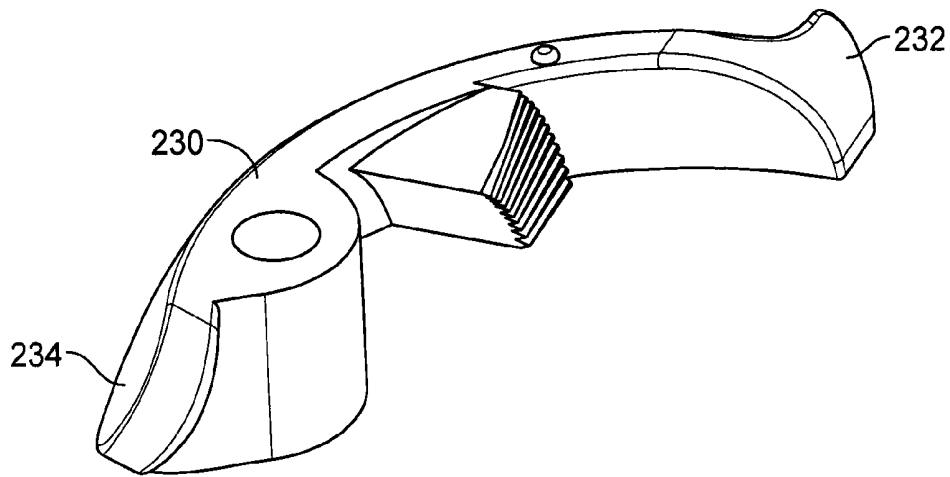


FIG. 38

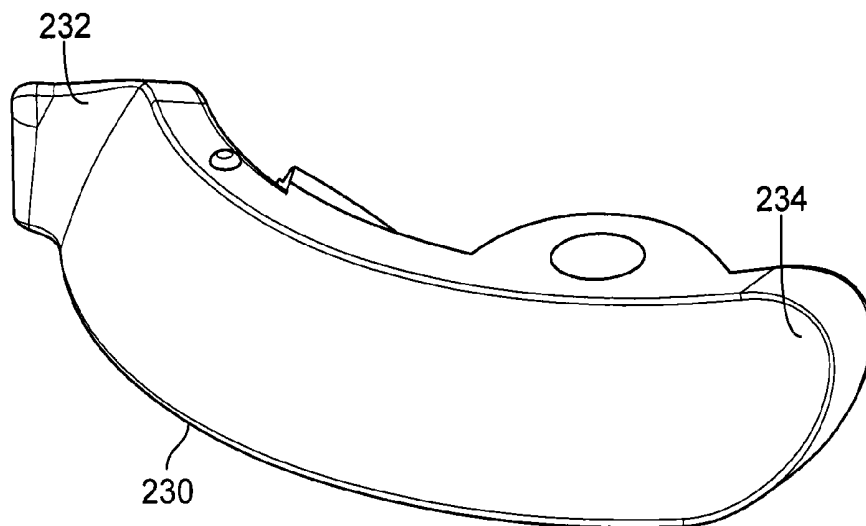


FIG. 39

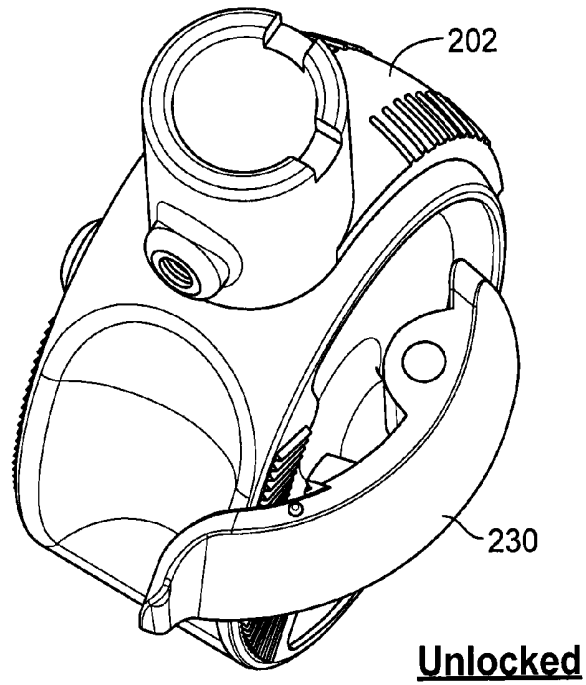


FIG. 40

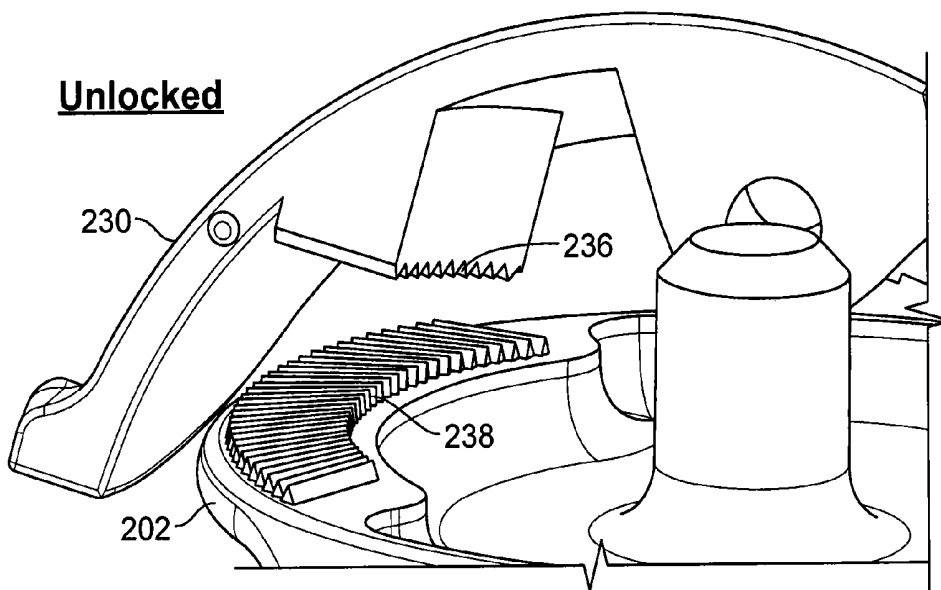


FIG. 41

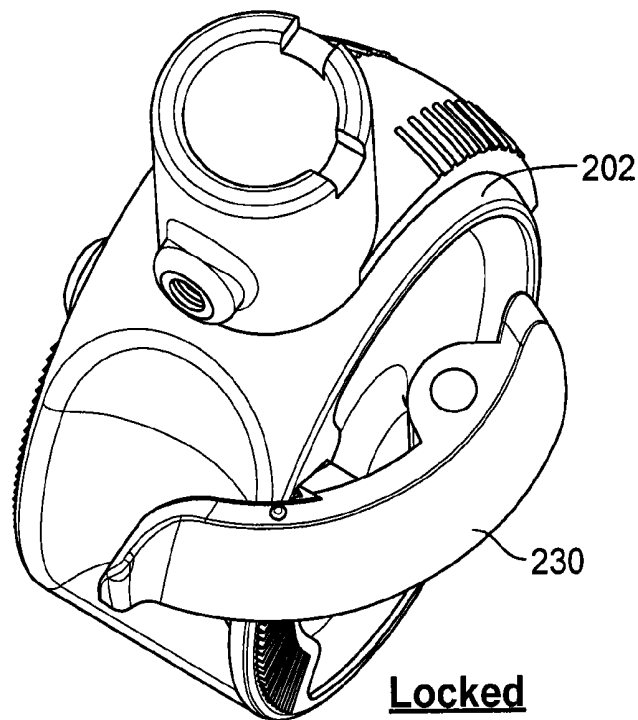


FIG. 42

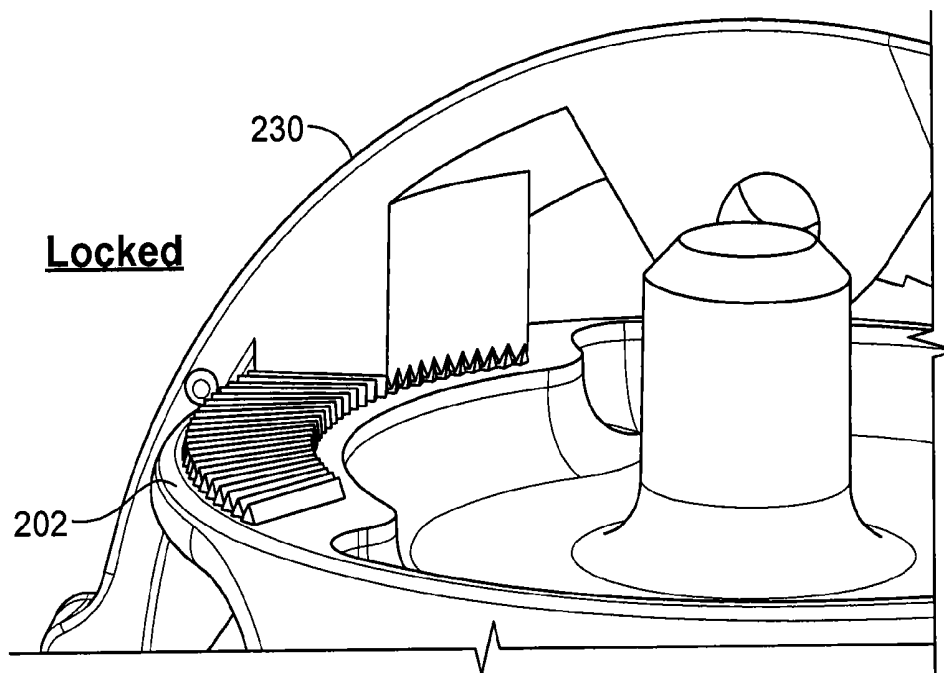


FIG. 43

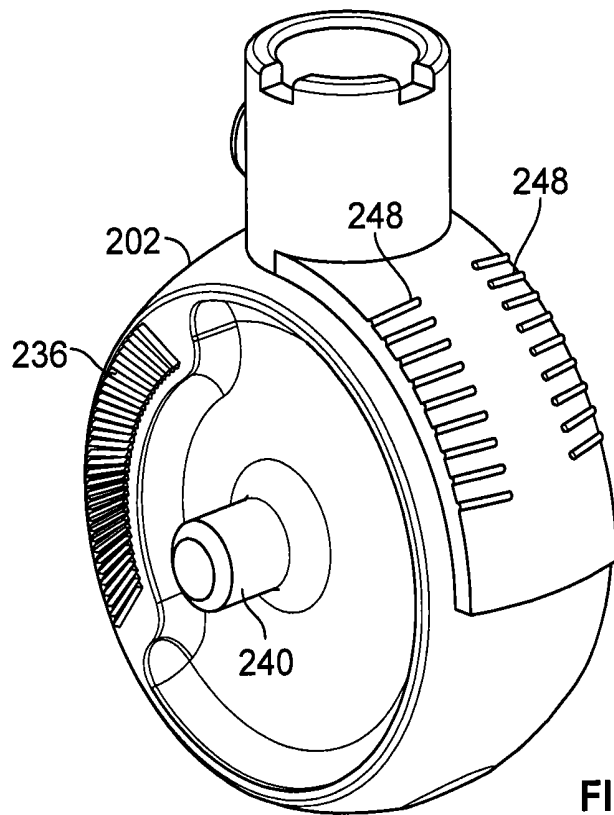


FIG. 44

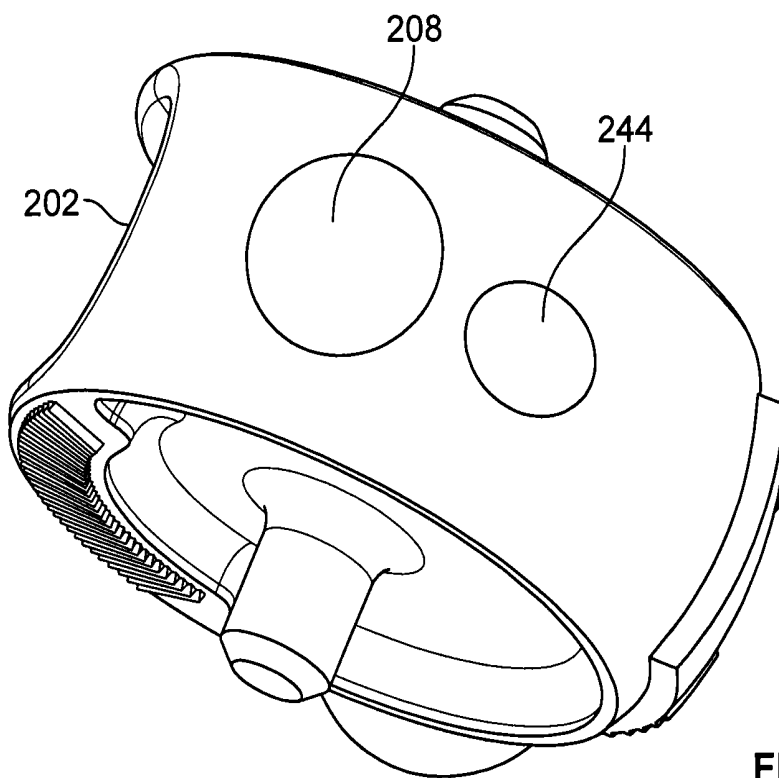
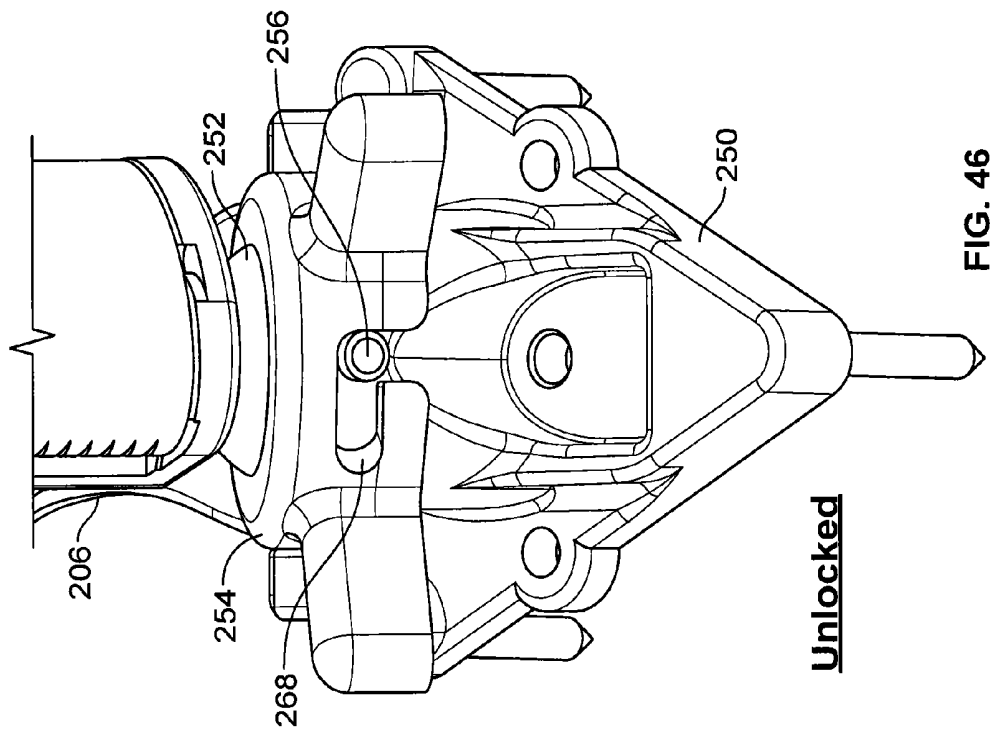
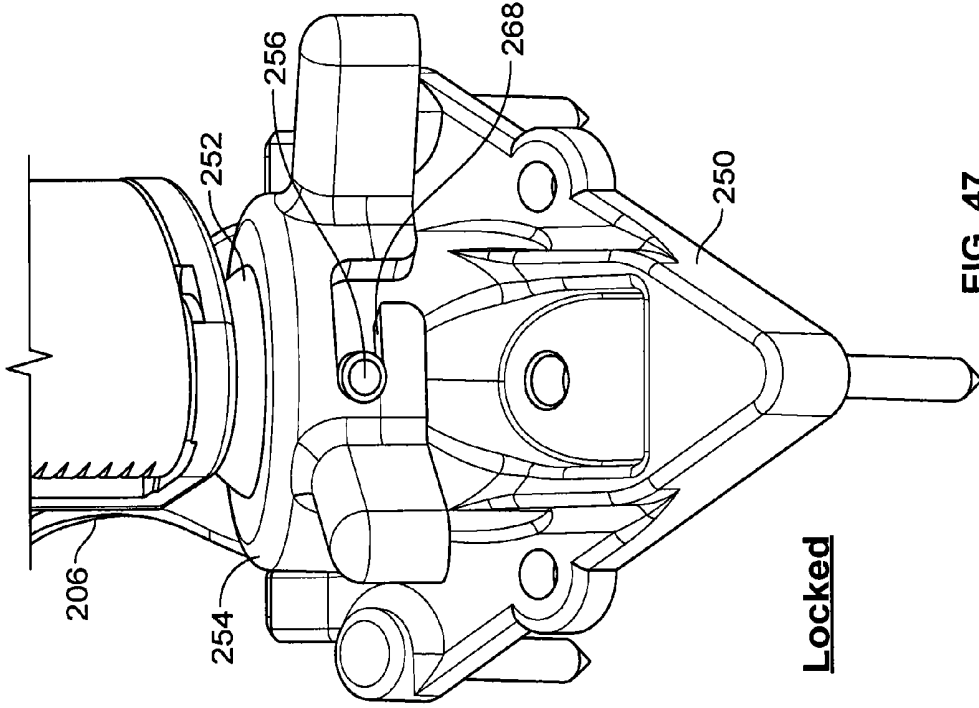


FIG. 45



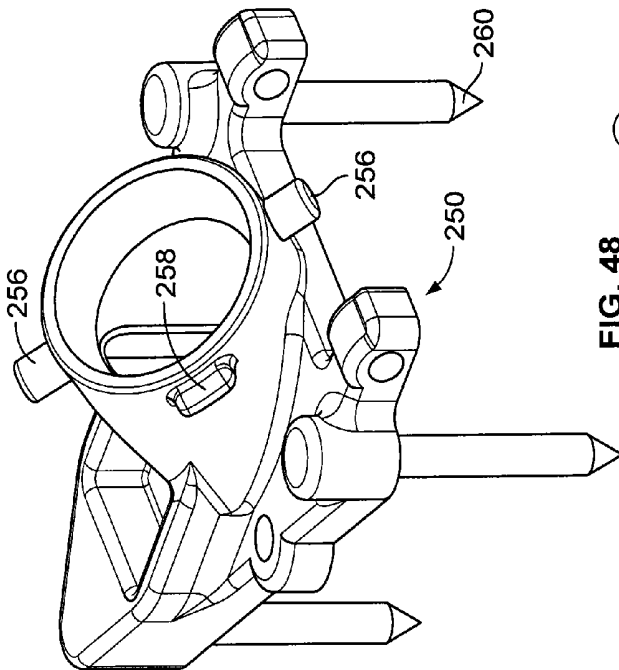


FIG. 48

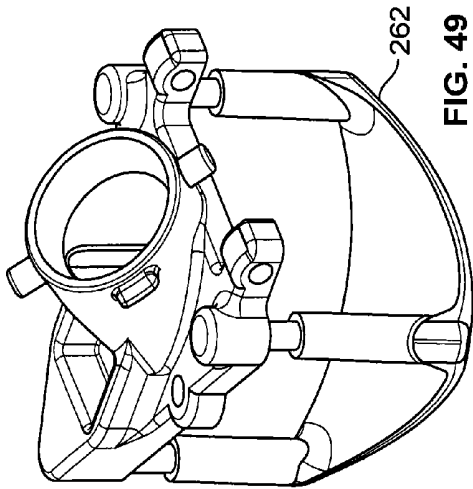


FIG. 49

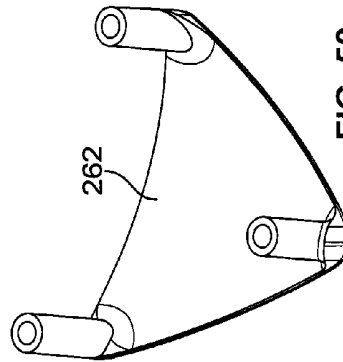


FIG. 50

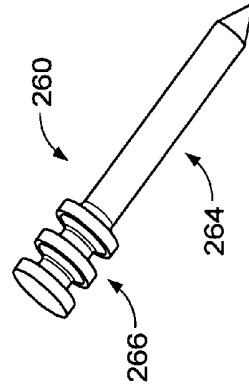


FIG. 51

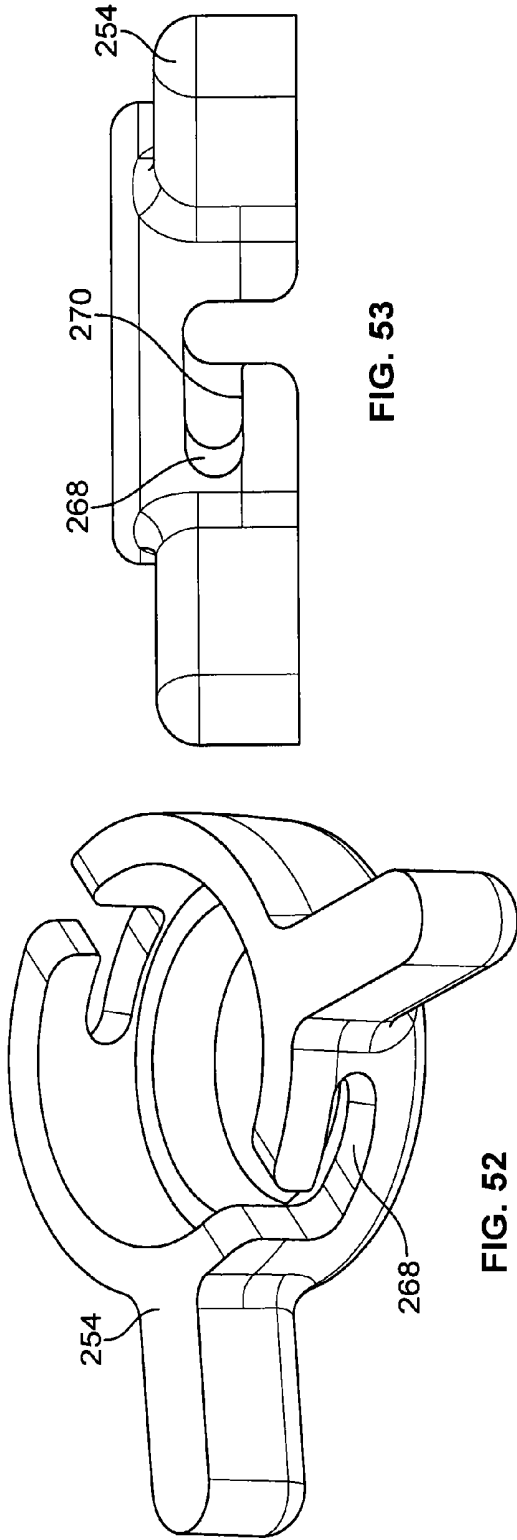


FIG. 53

FIG. 52

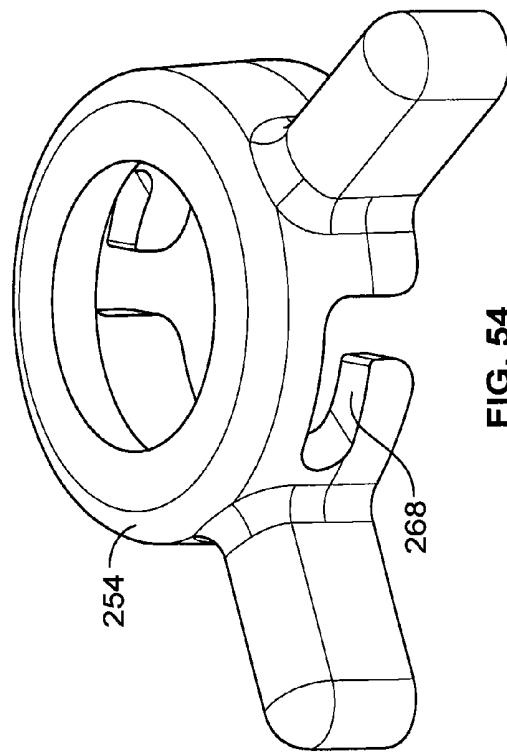


FIG. 54

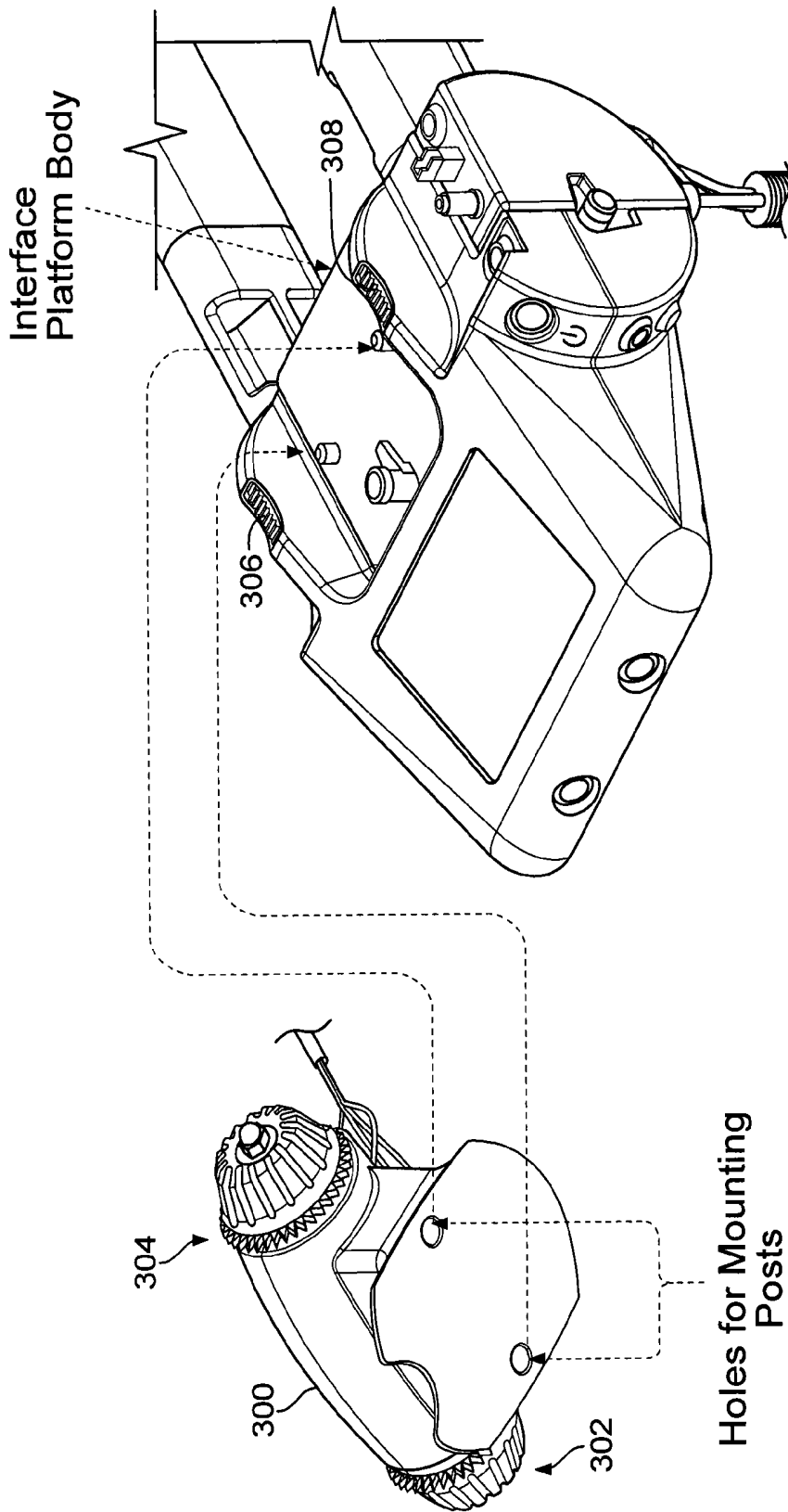


FIG. 55

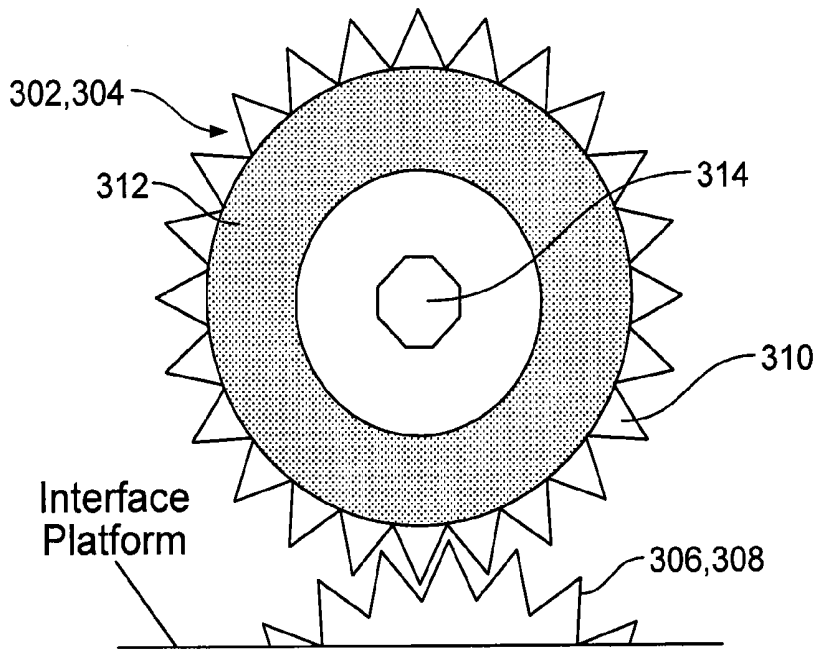


FIG. 56

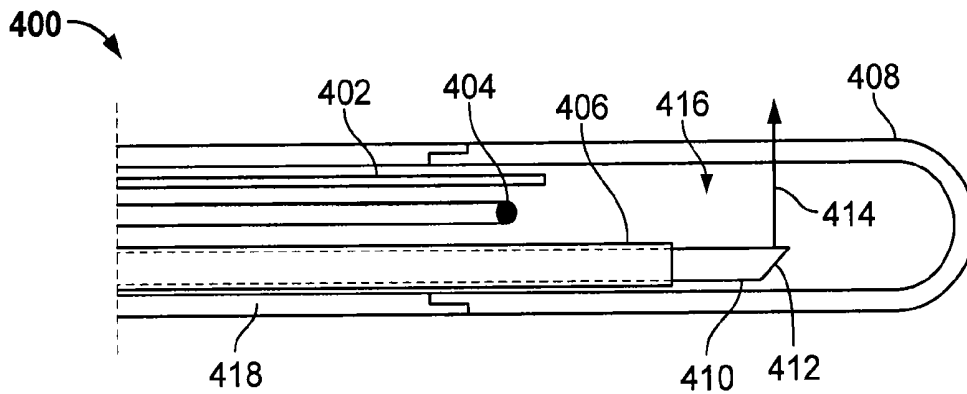


FIG. 57

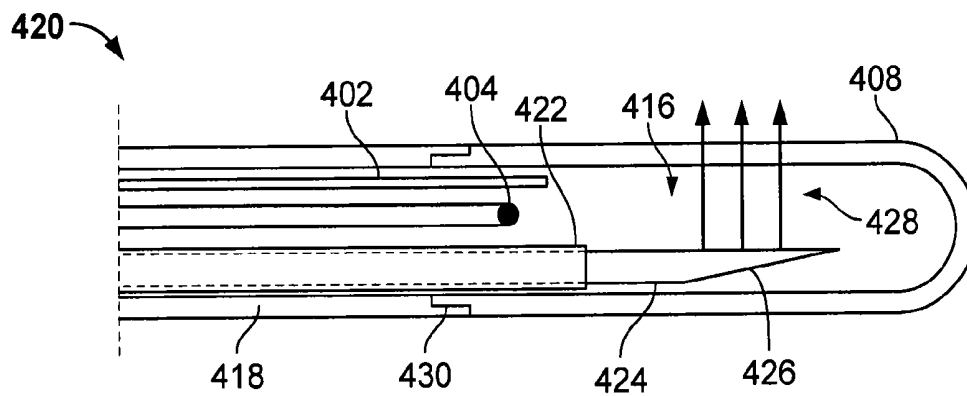


FIG. 58

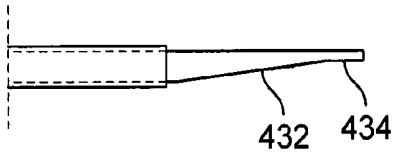


FIG. 59

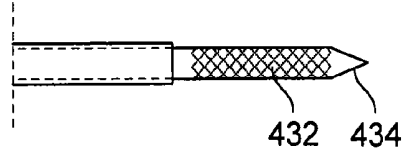


FIG. 60

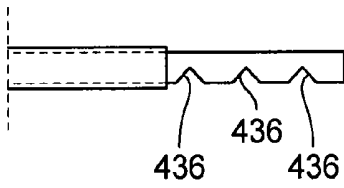


FIG. 61

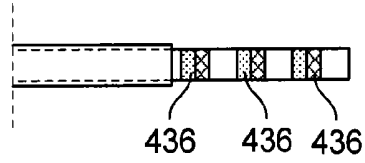


FIG. 62

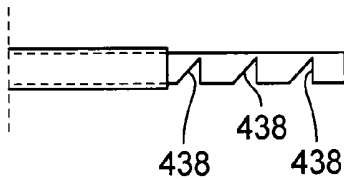


FIG. 63

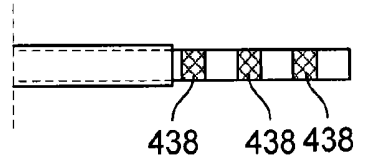


FIG. 64

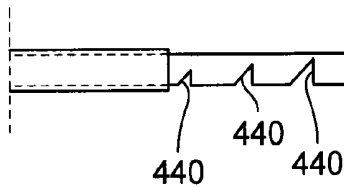


FIG. 65

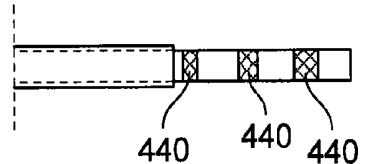


FIG. 66

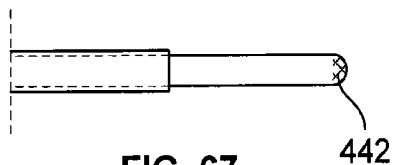


FIG. 67

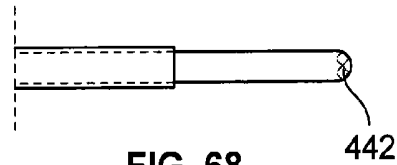


FIG. 68

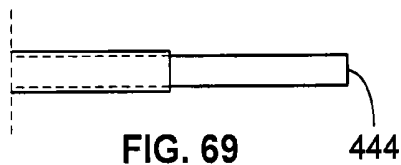


FIG. 69

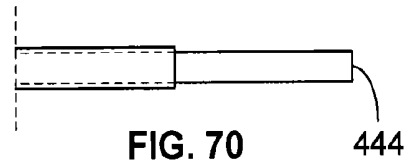


FIG. 70

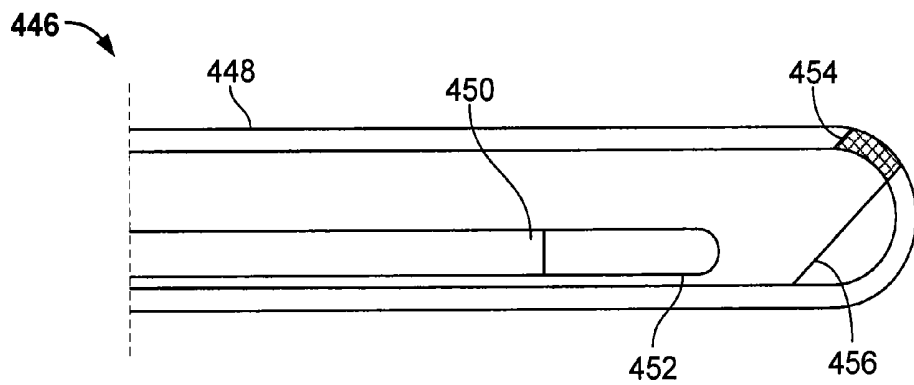


FIG. 71A

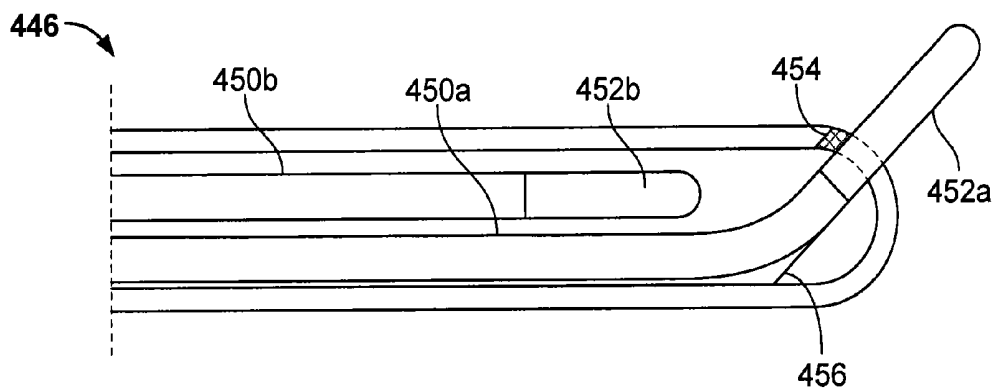


FIG. 71B

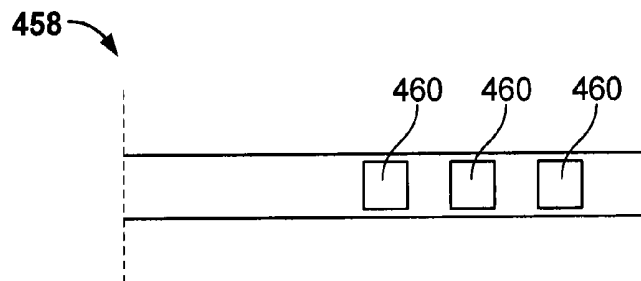


FIG. 72

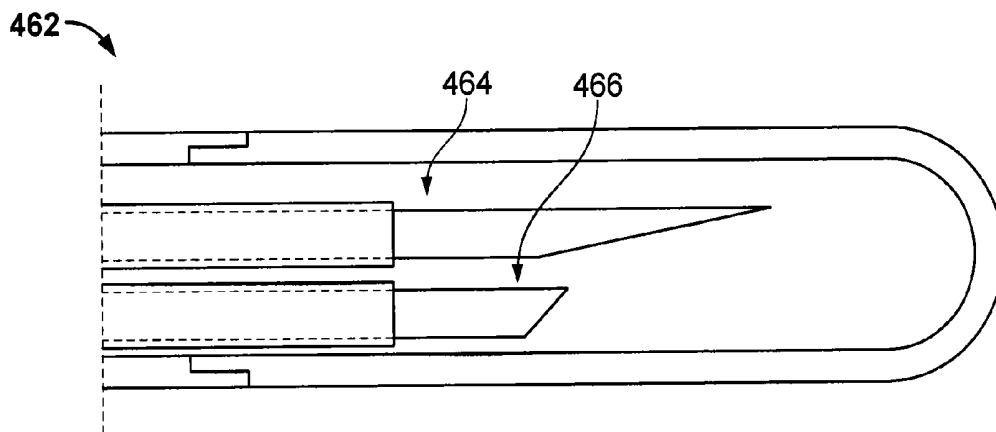


FIG. 73

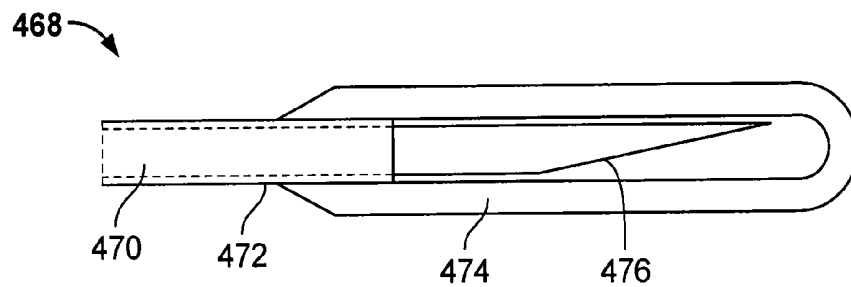
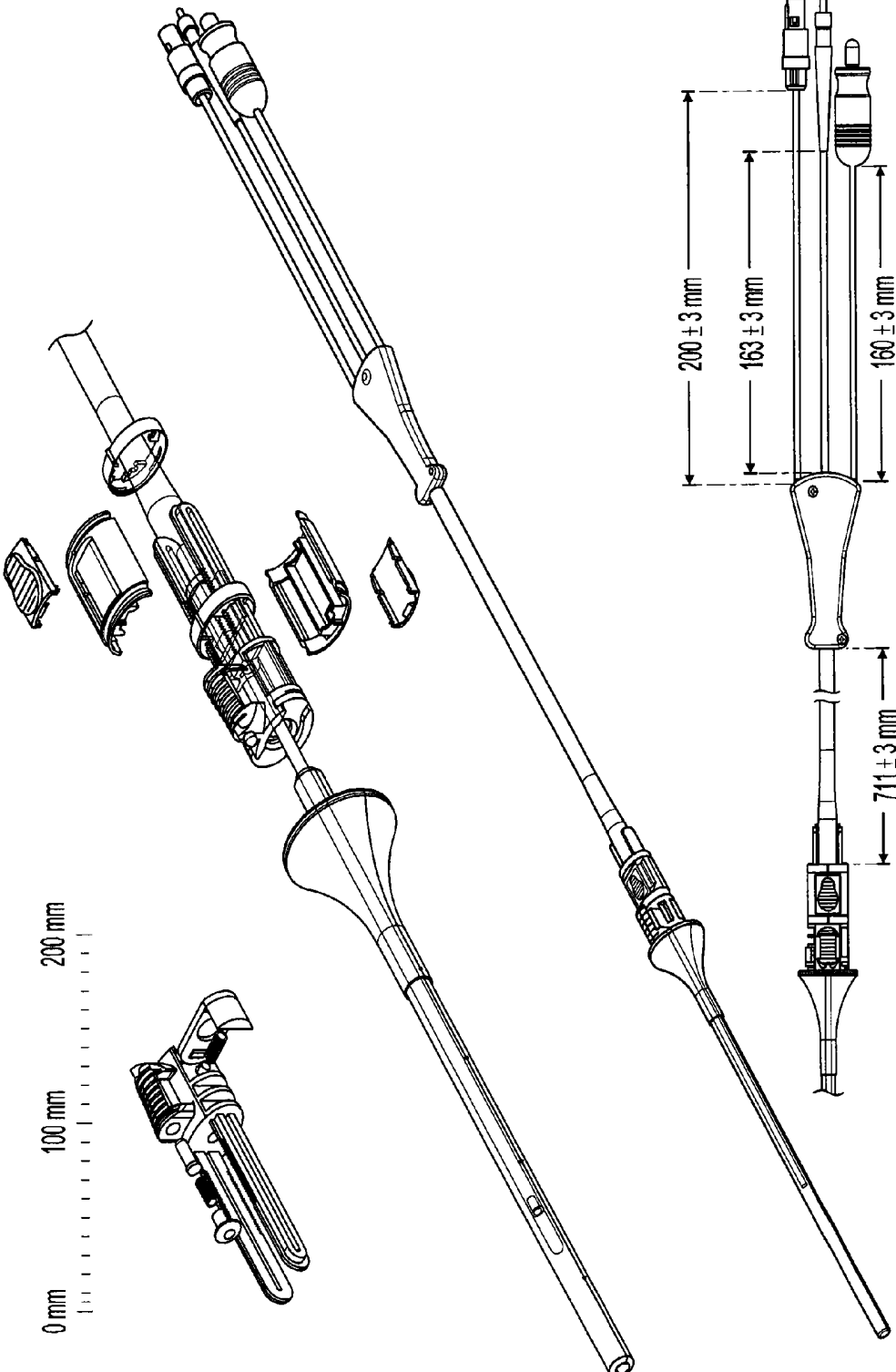


FIG. 74



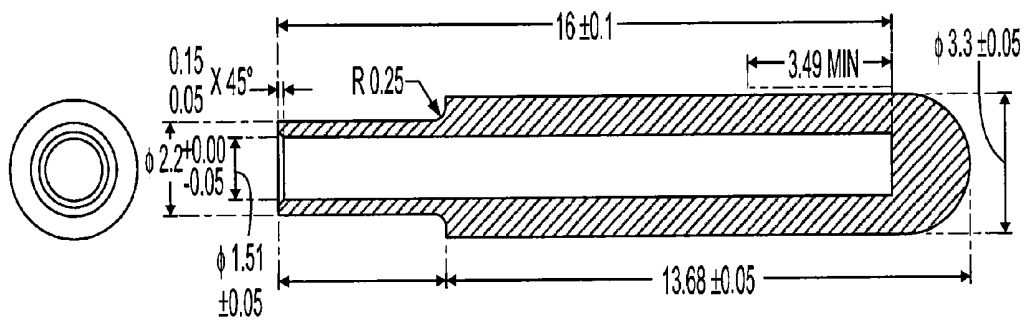


FIG. 76

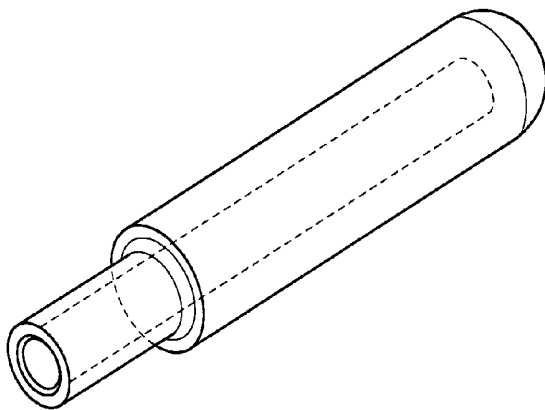
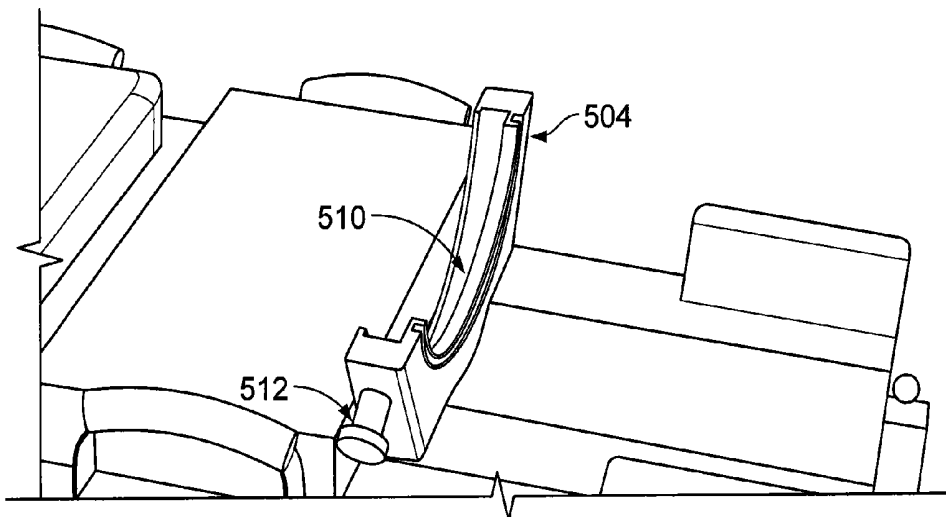
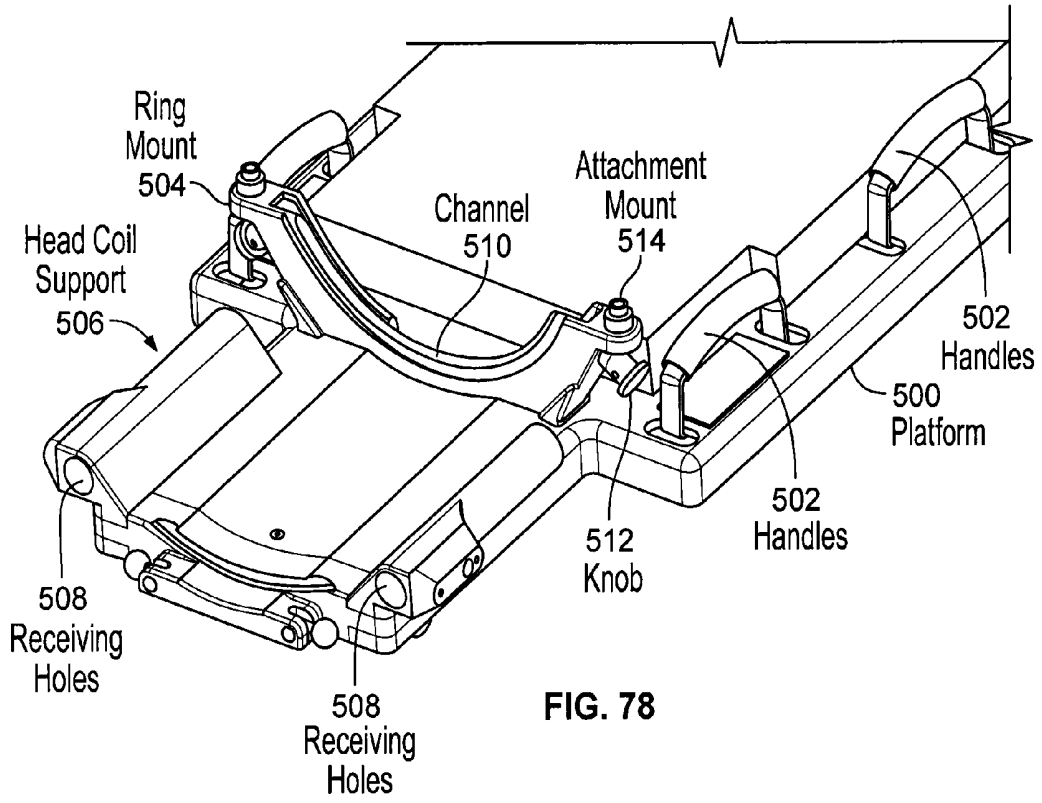


FIG. 77



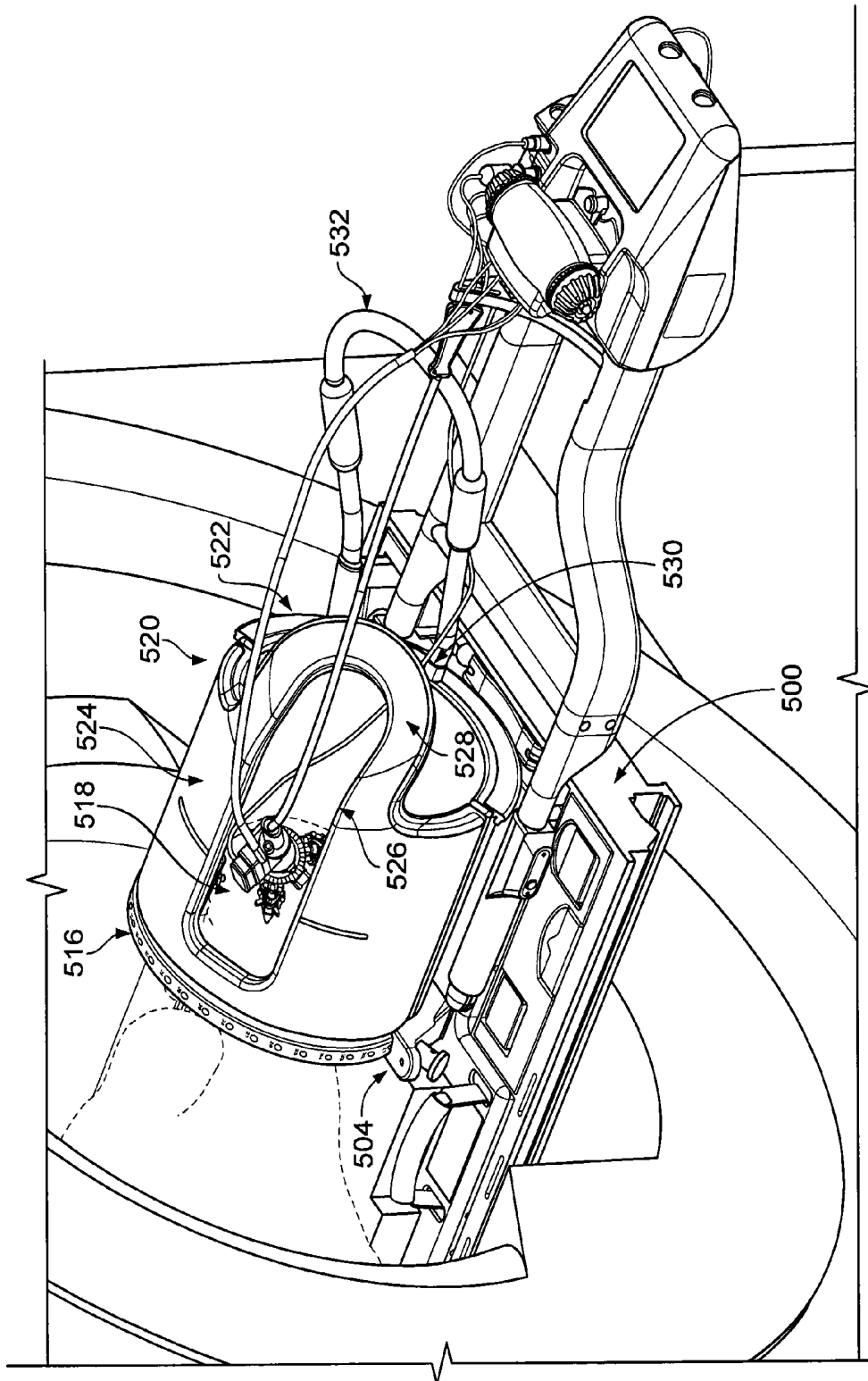


FIG. 80

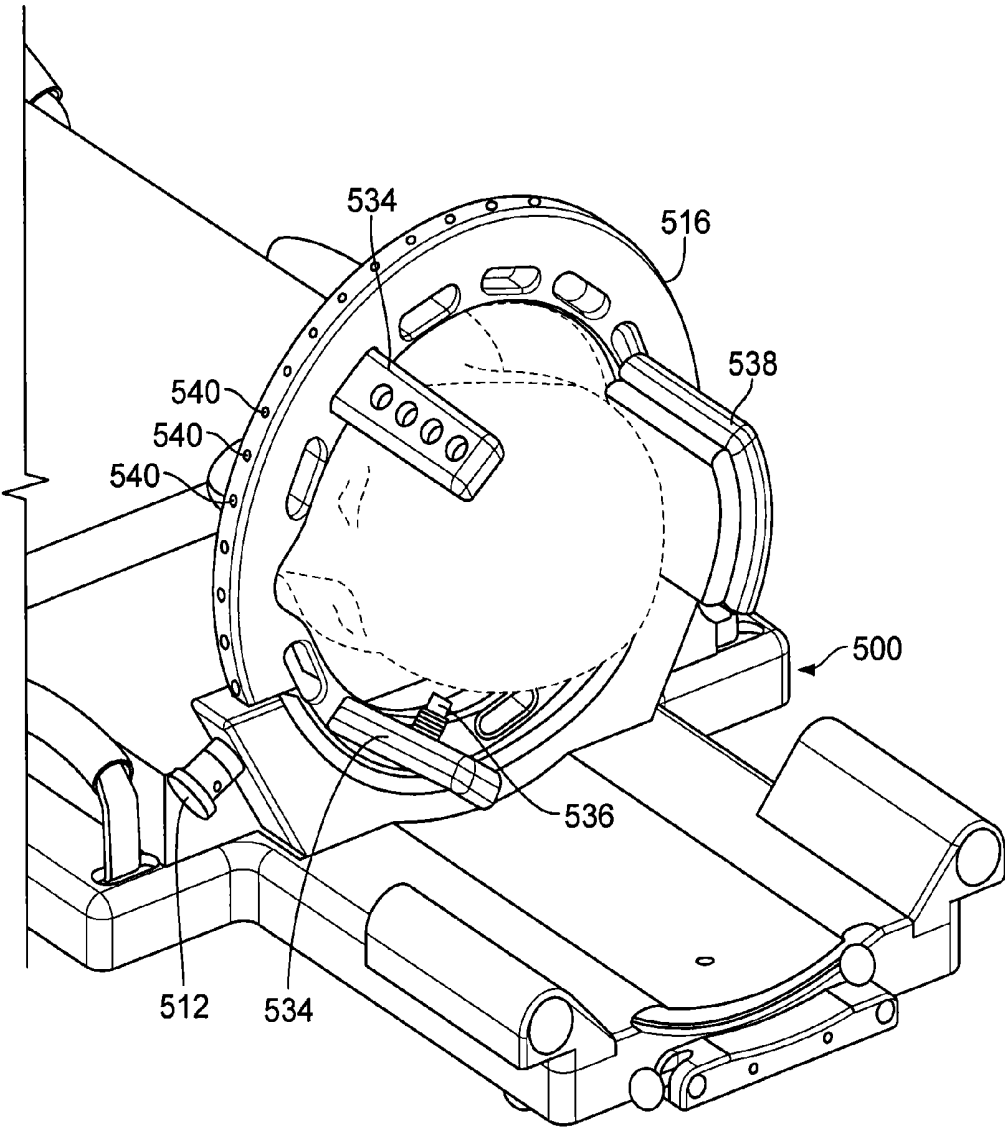


FIG. 81

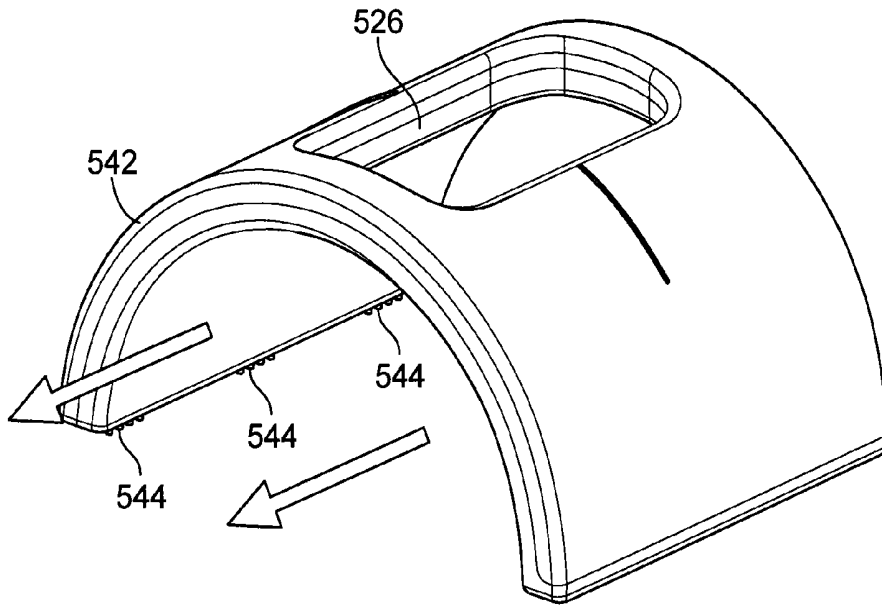


FIG. 82

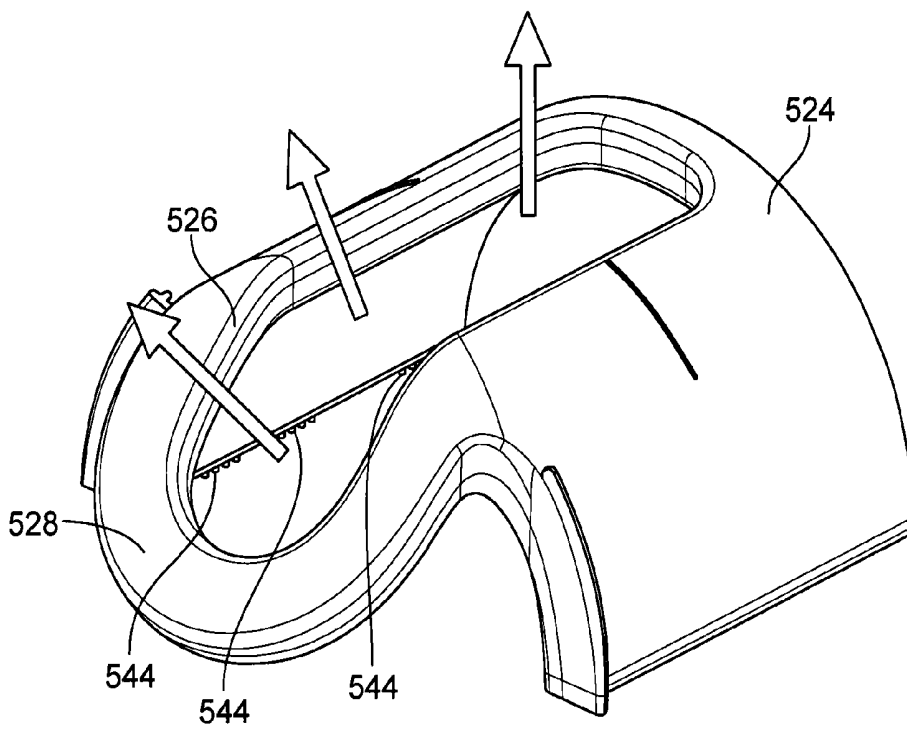


FIG. 83

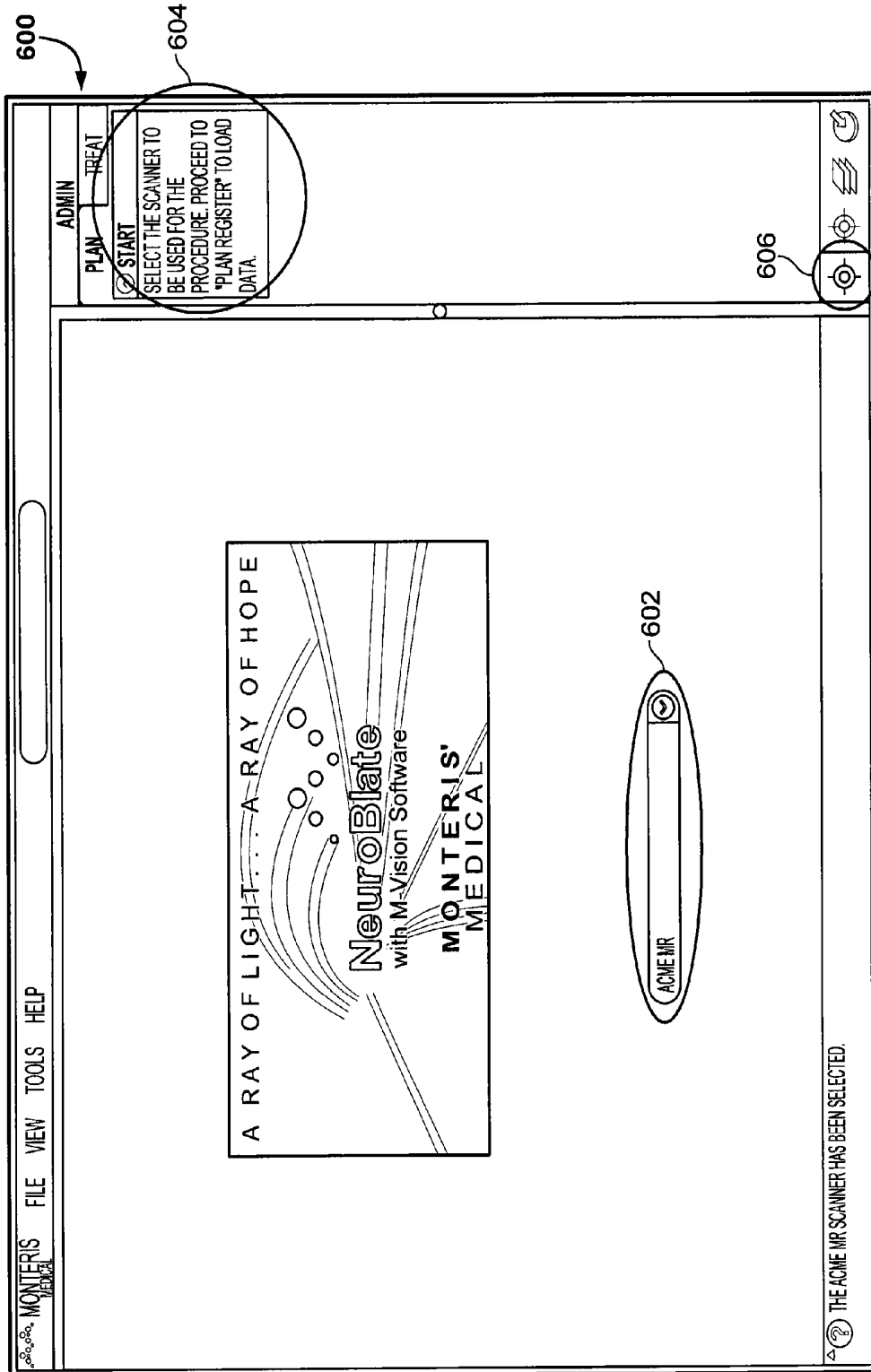


FIG. 84

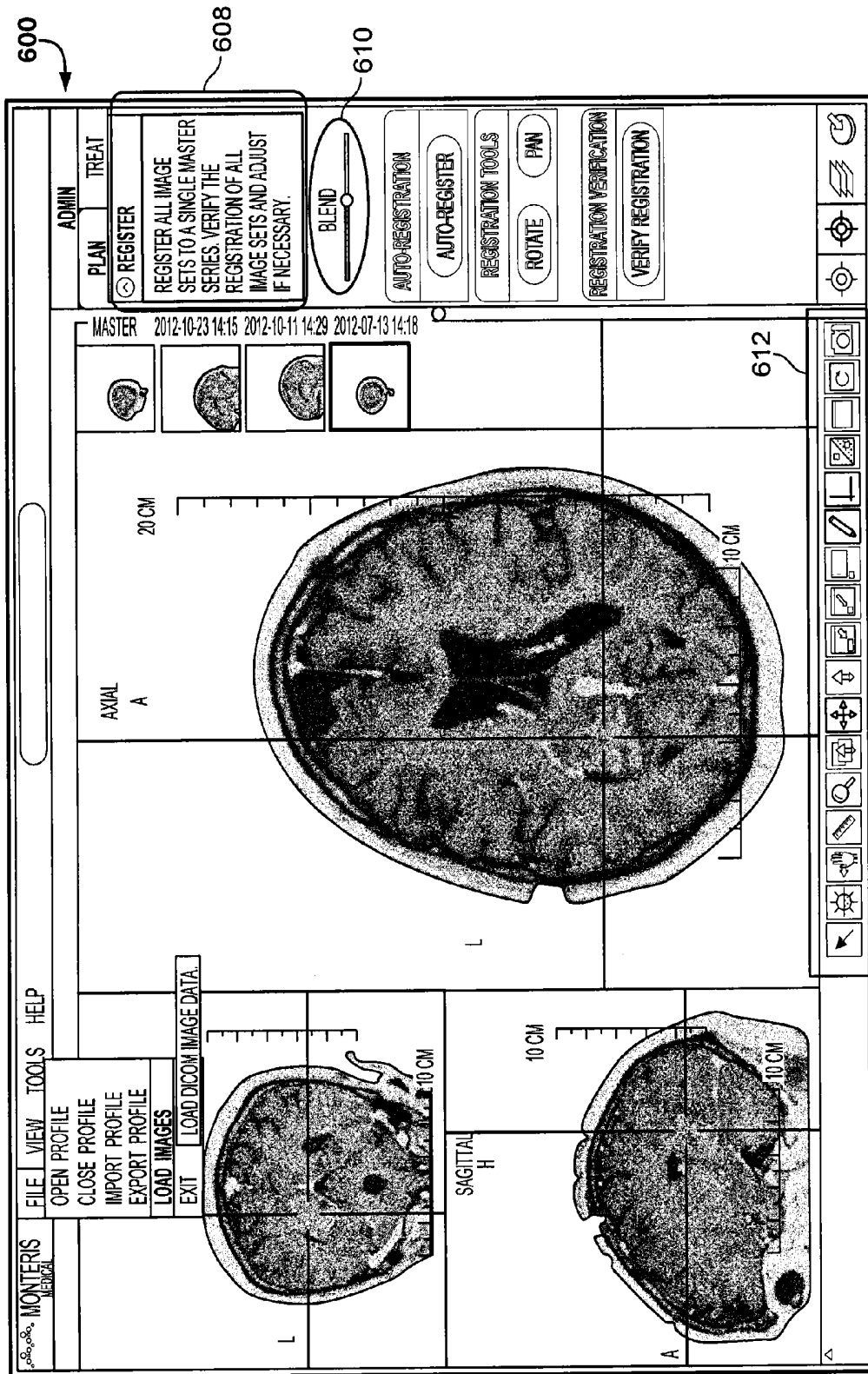


FIG. 85

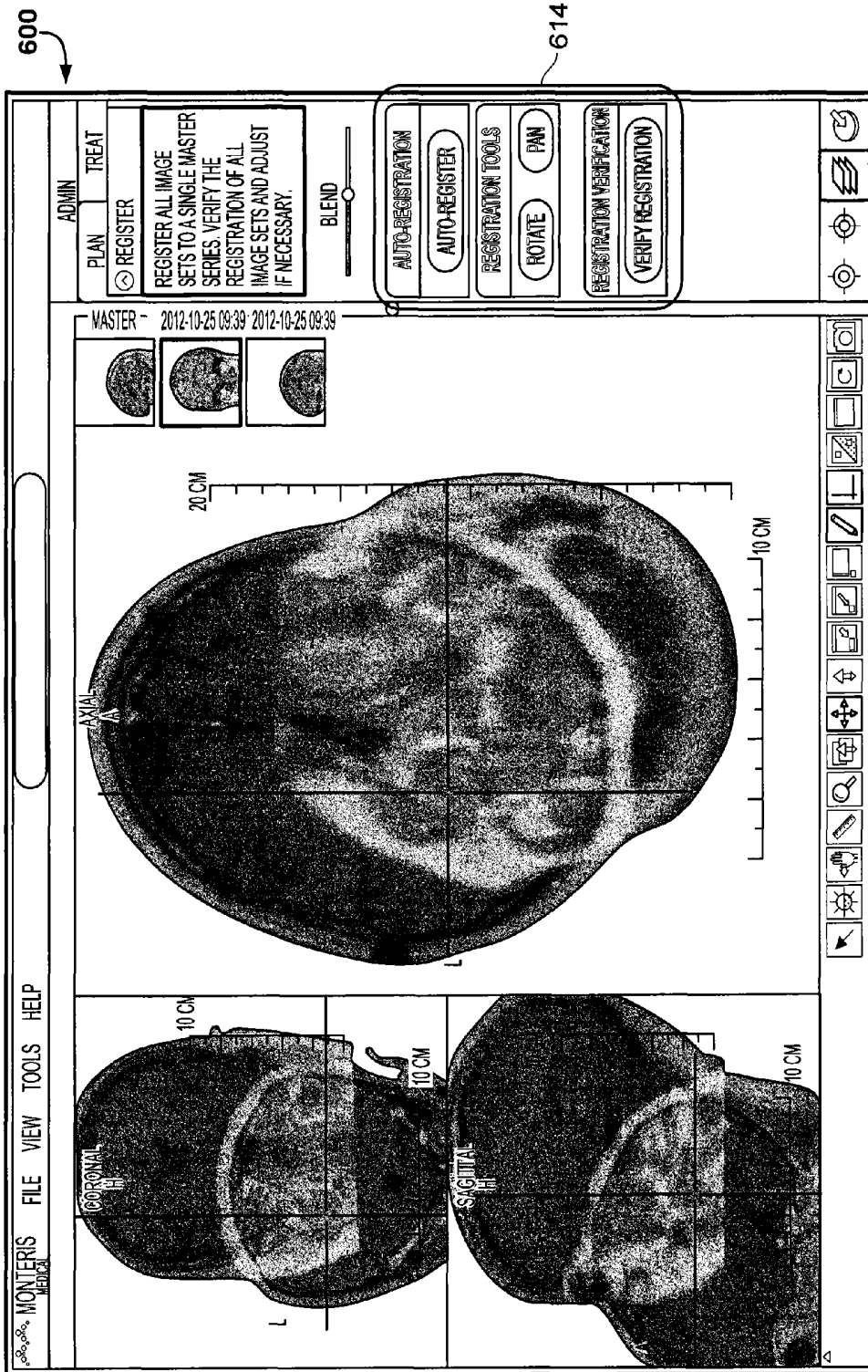


FIG. 86

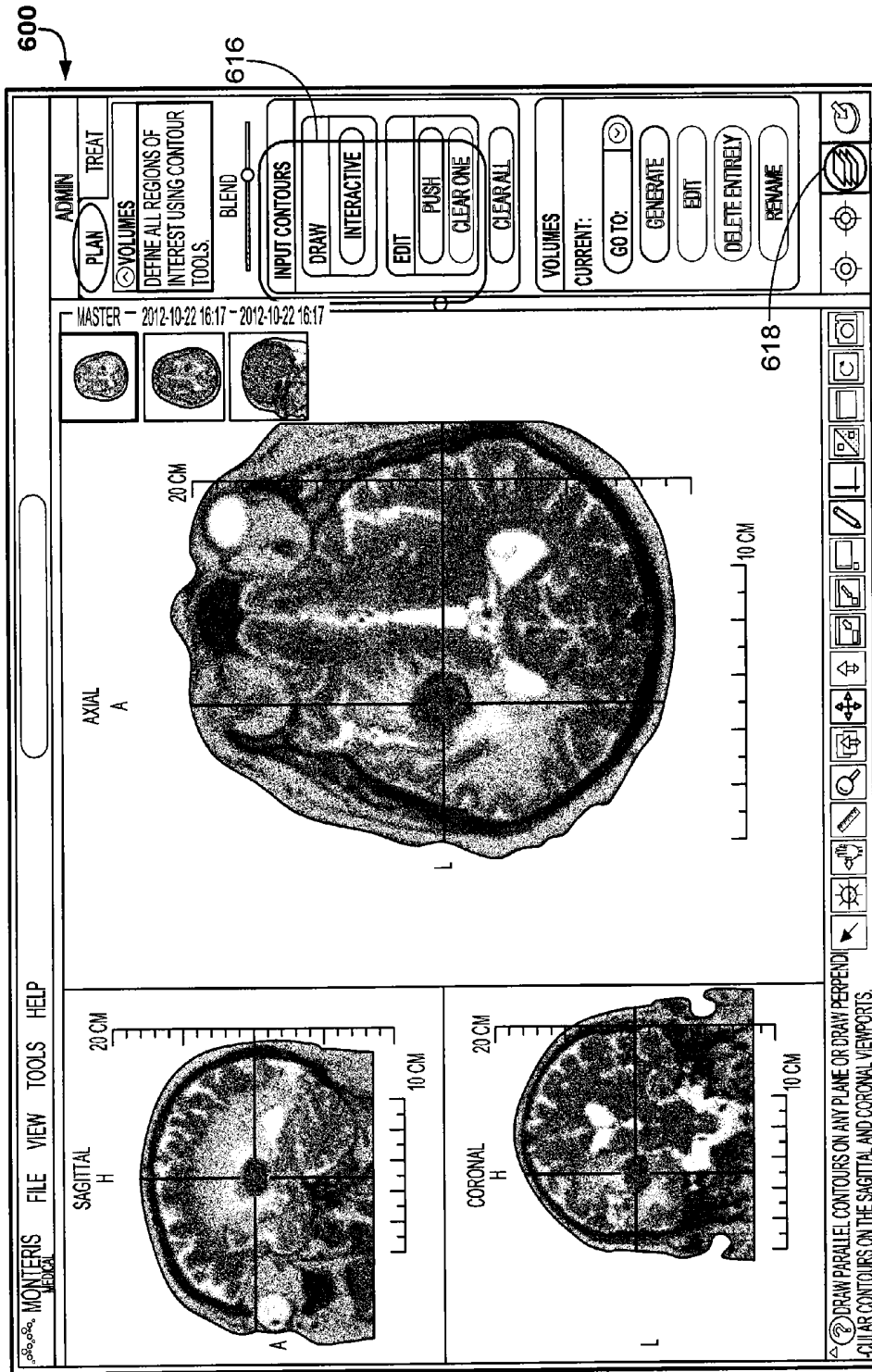


FIG. 87

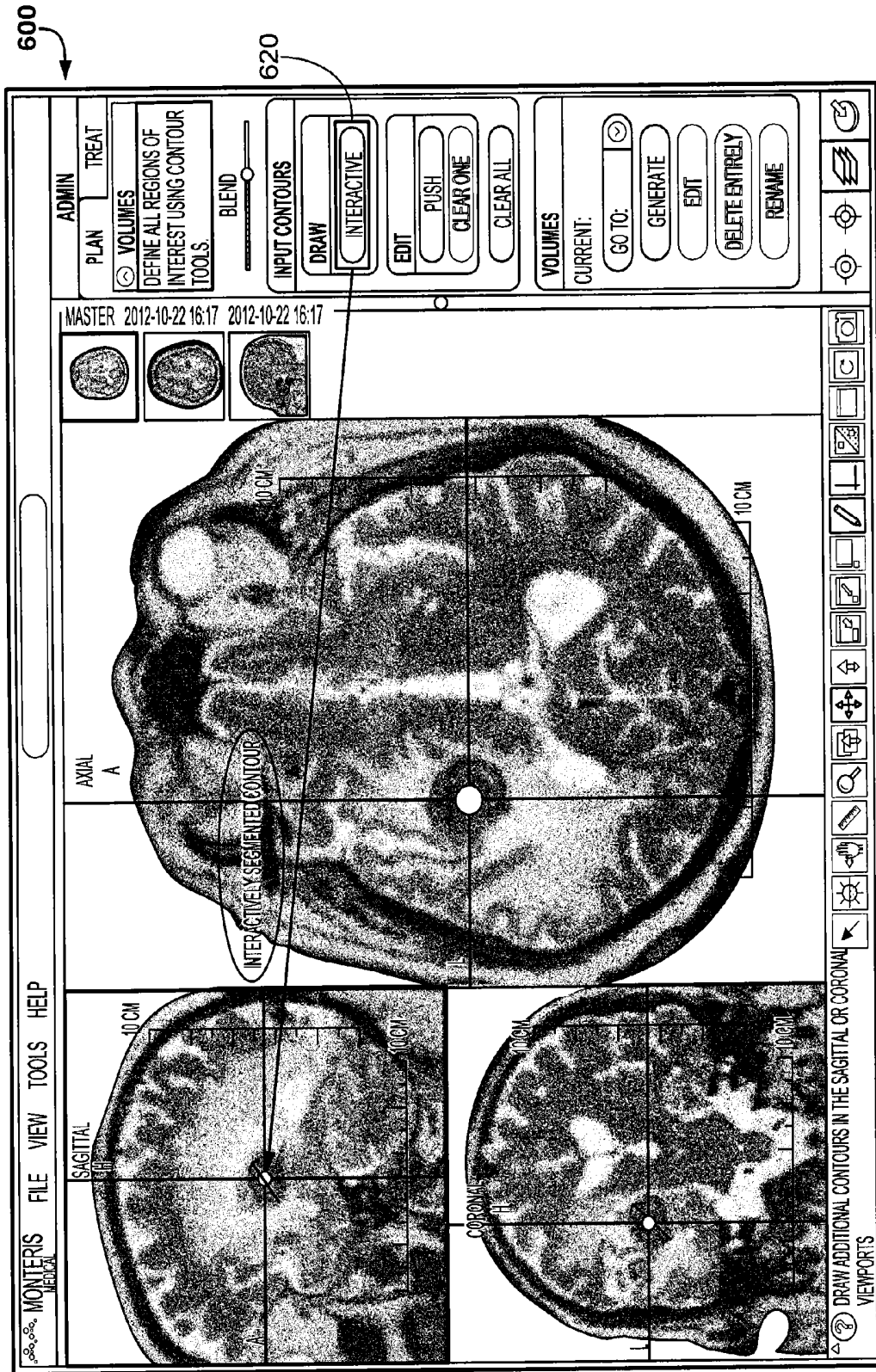


FIG. 88

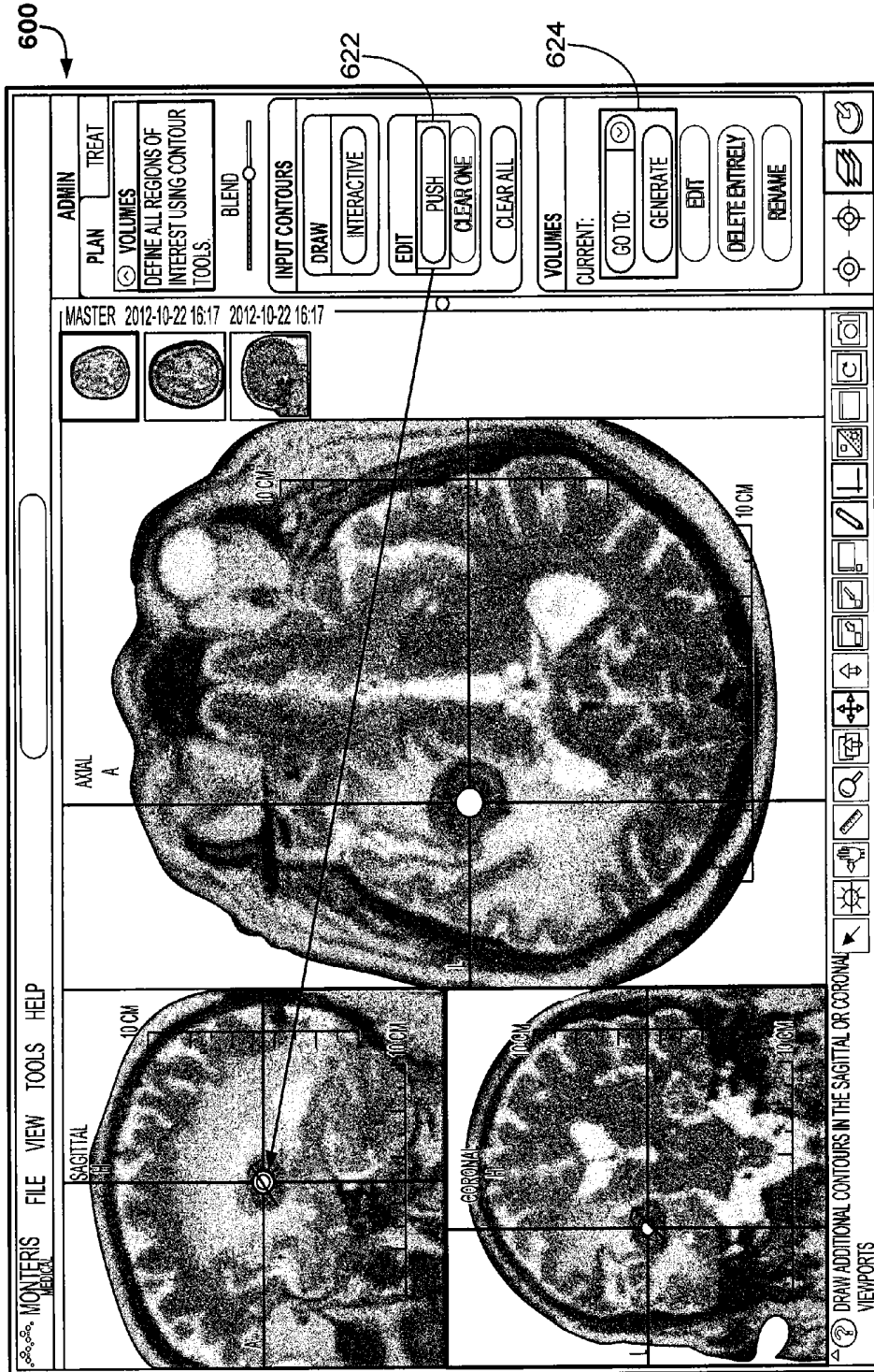


FIG. 89

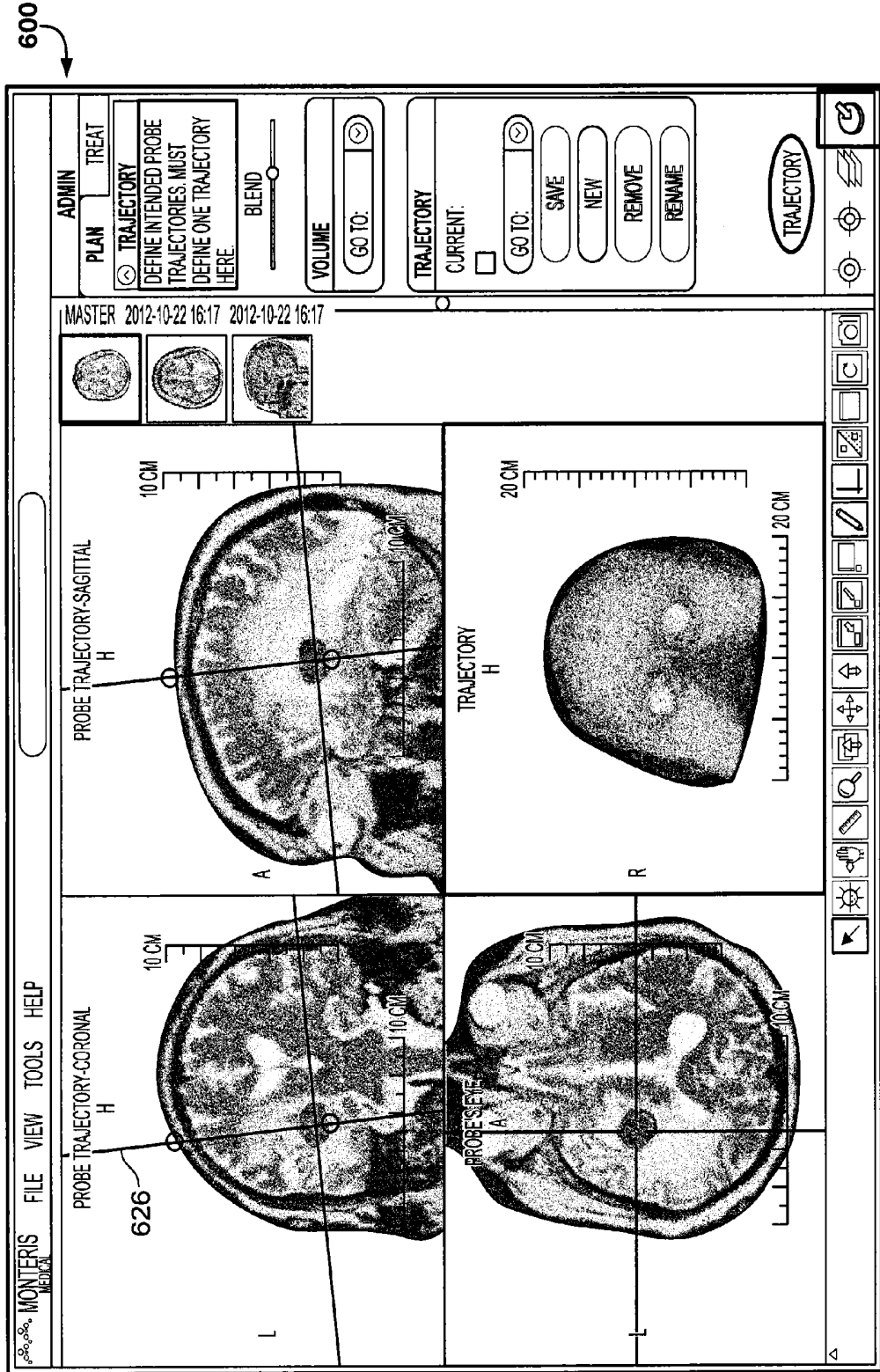


FIG. 90

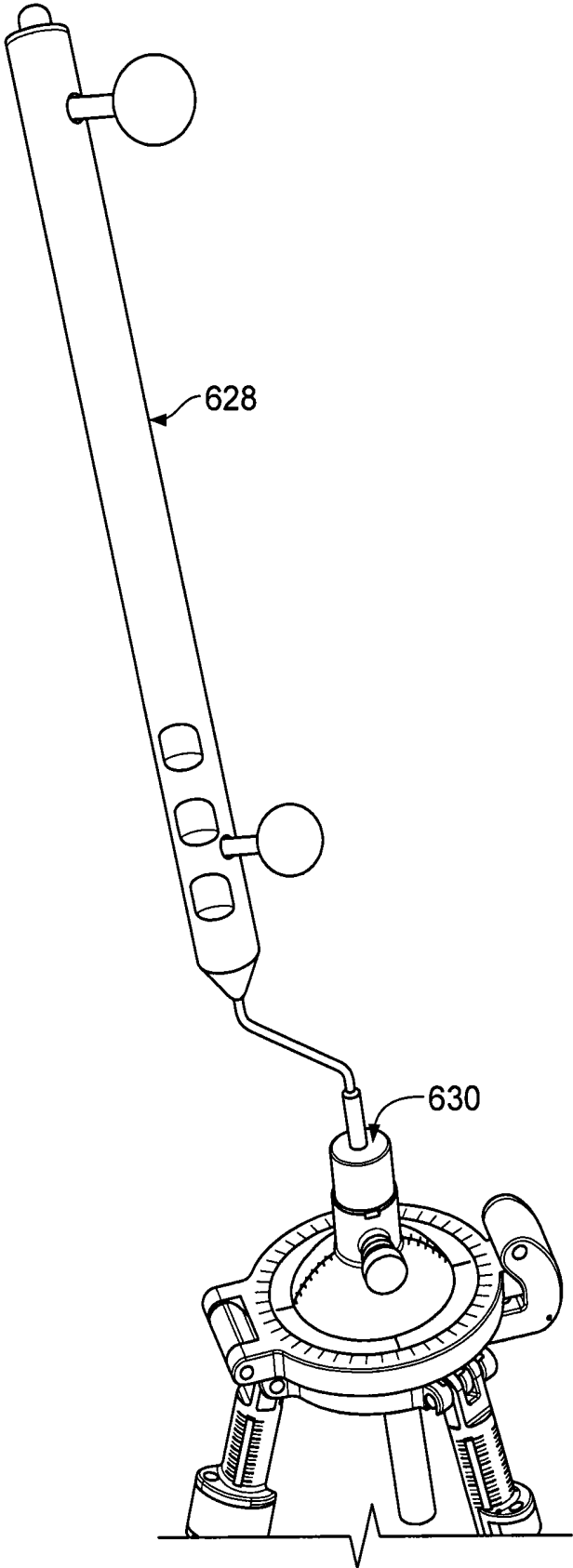


FIG. 91

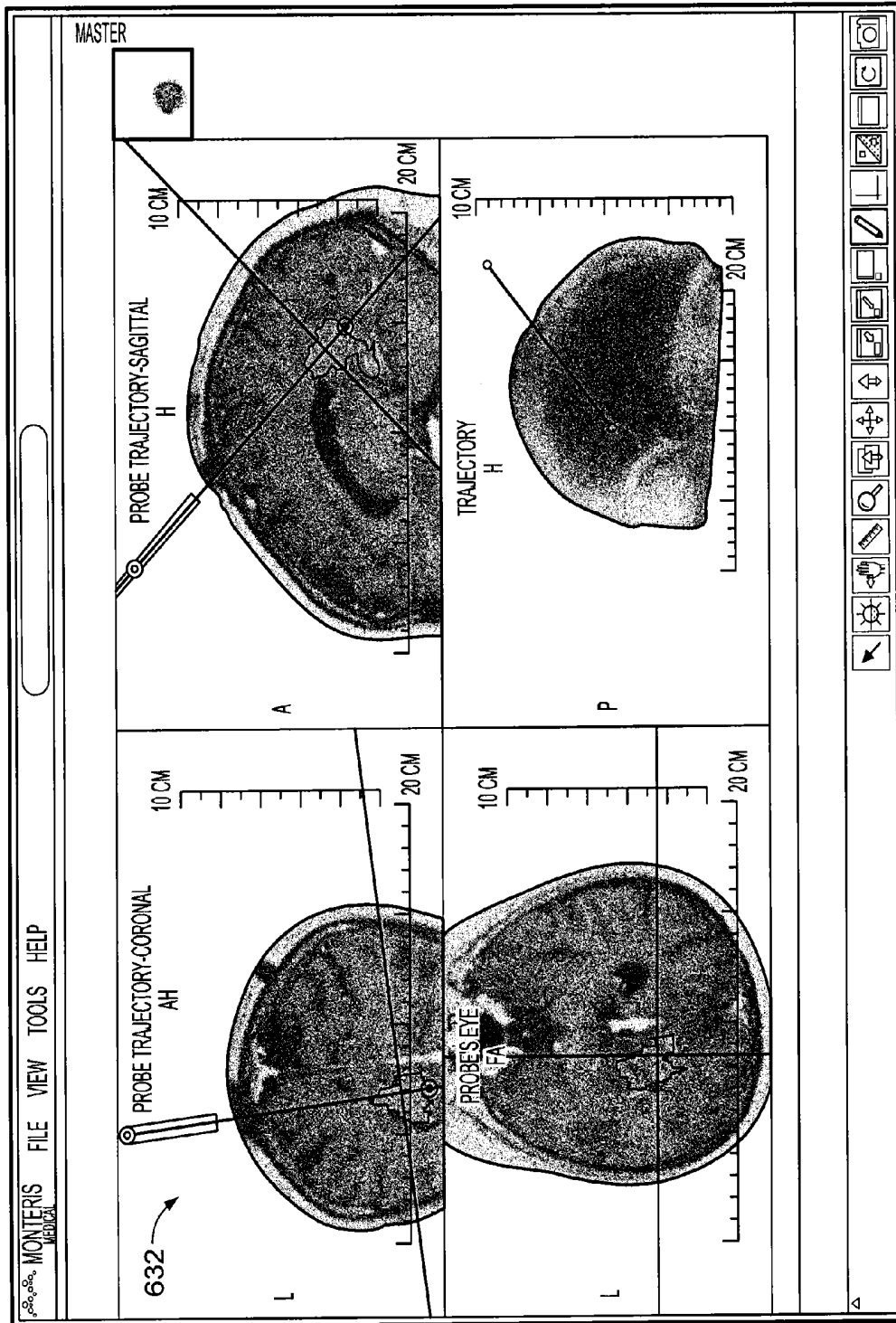


FIG. 92

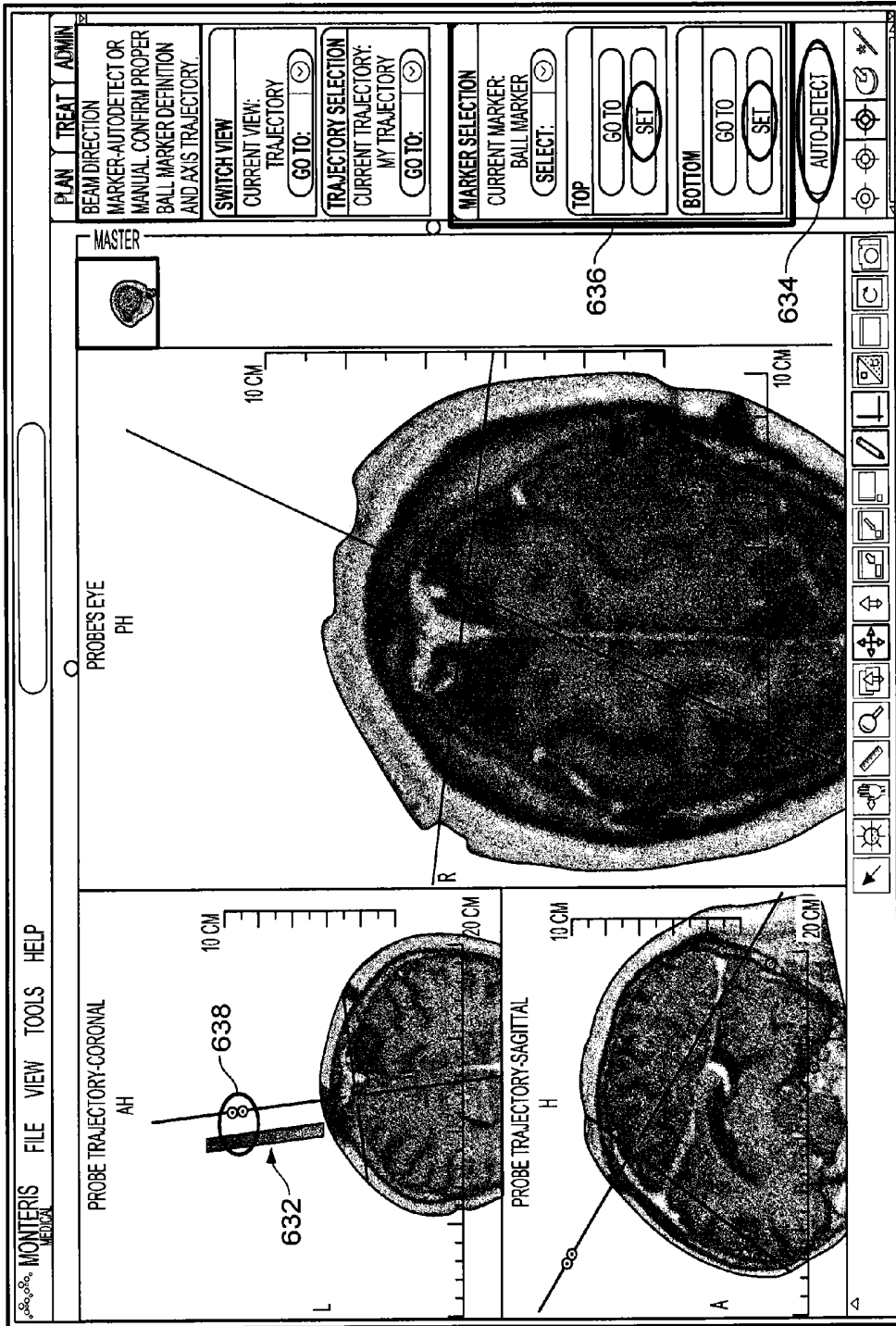


FIG. 93

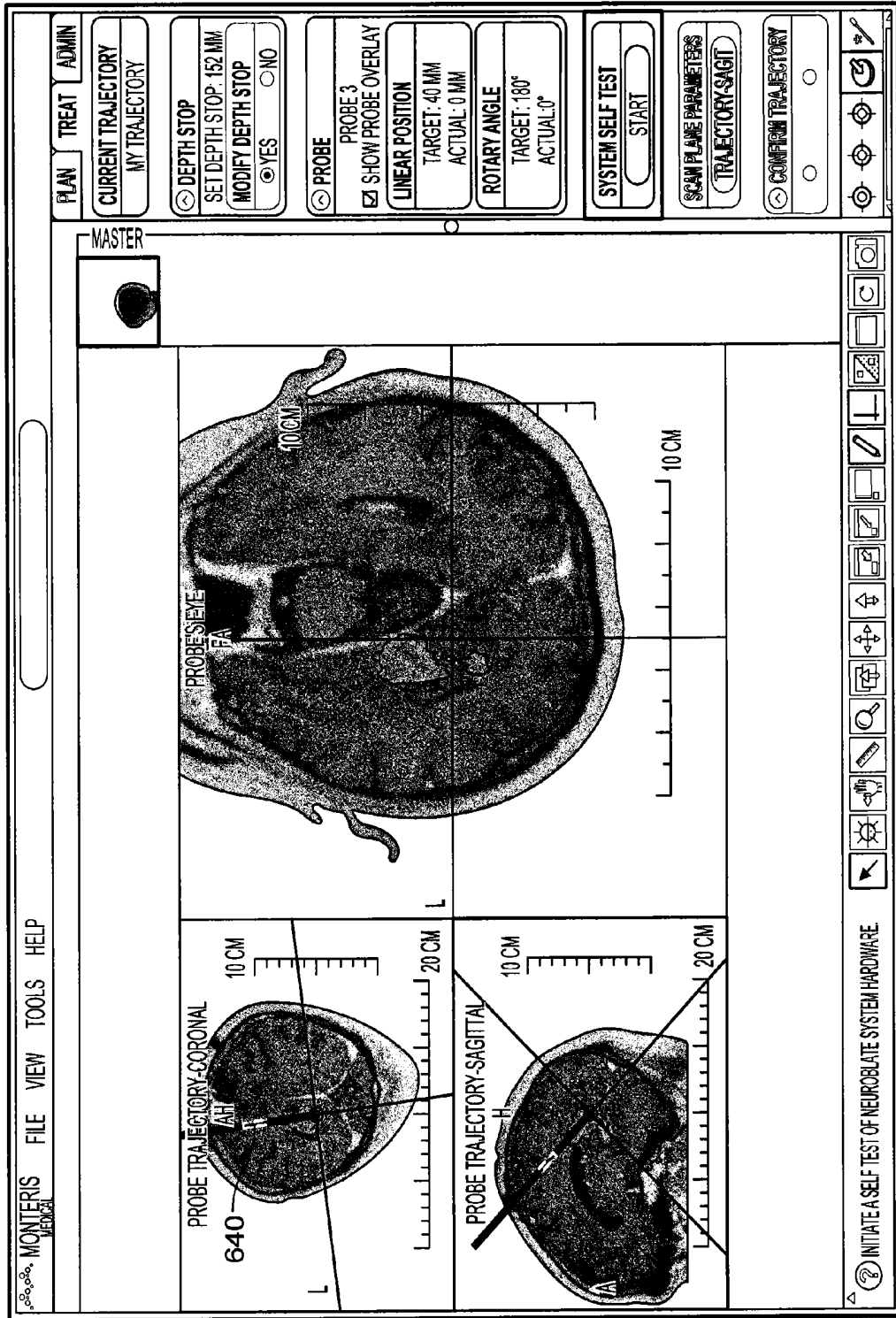
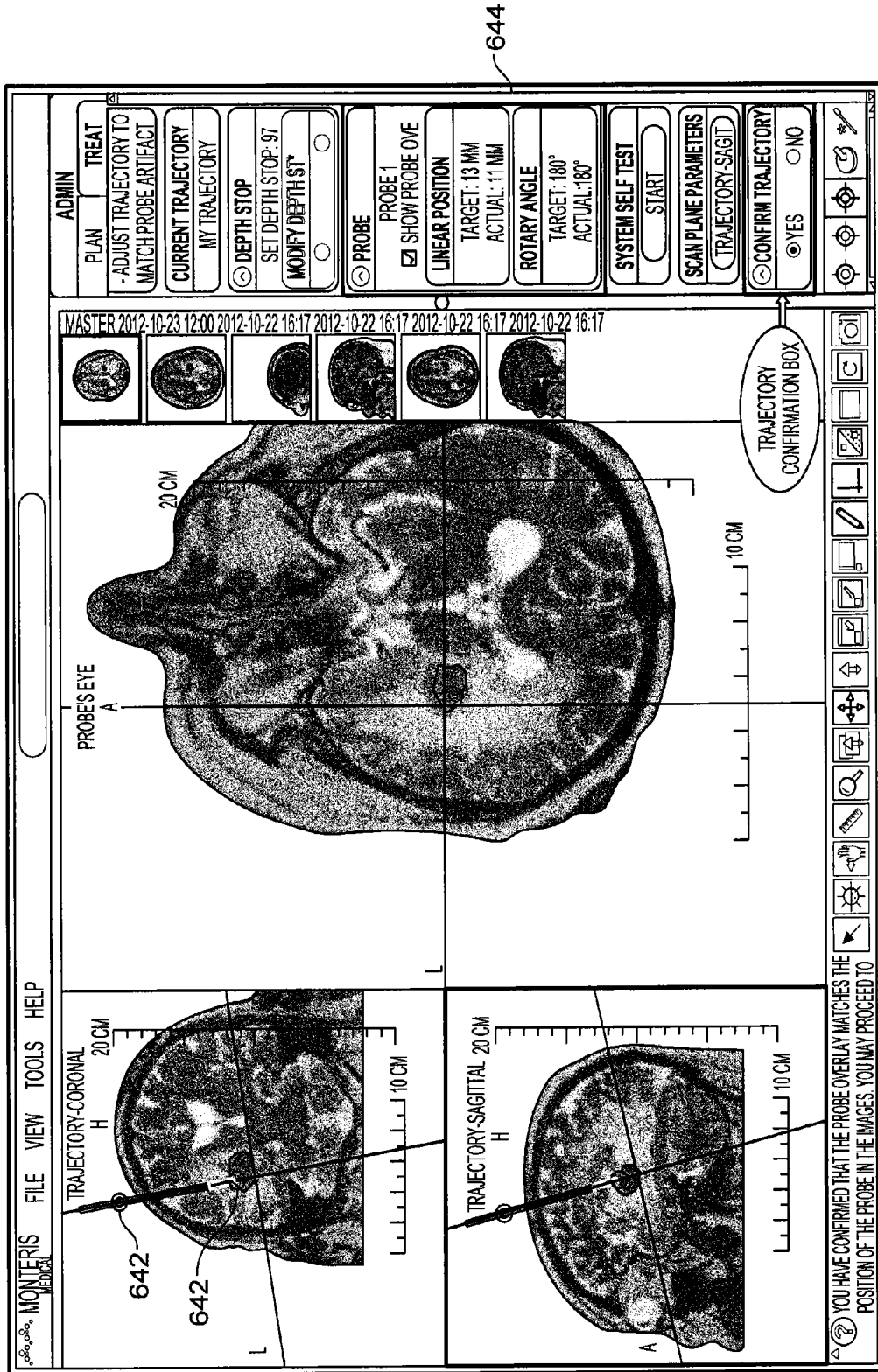


FIG. 94



644

FIG. 95

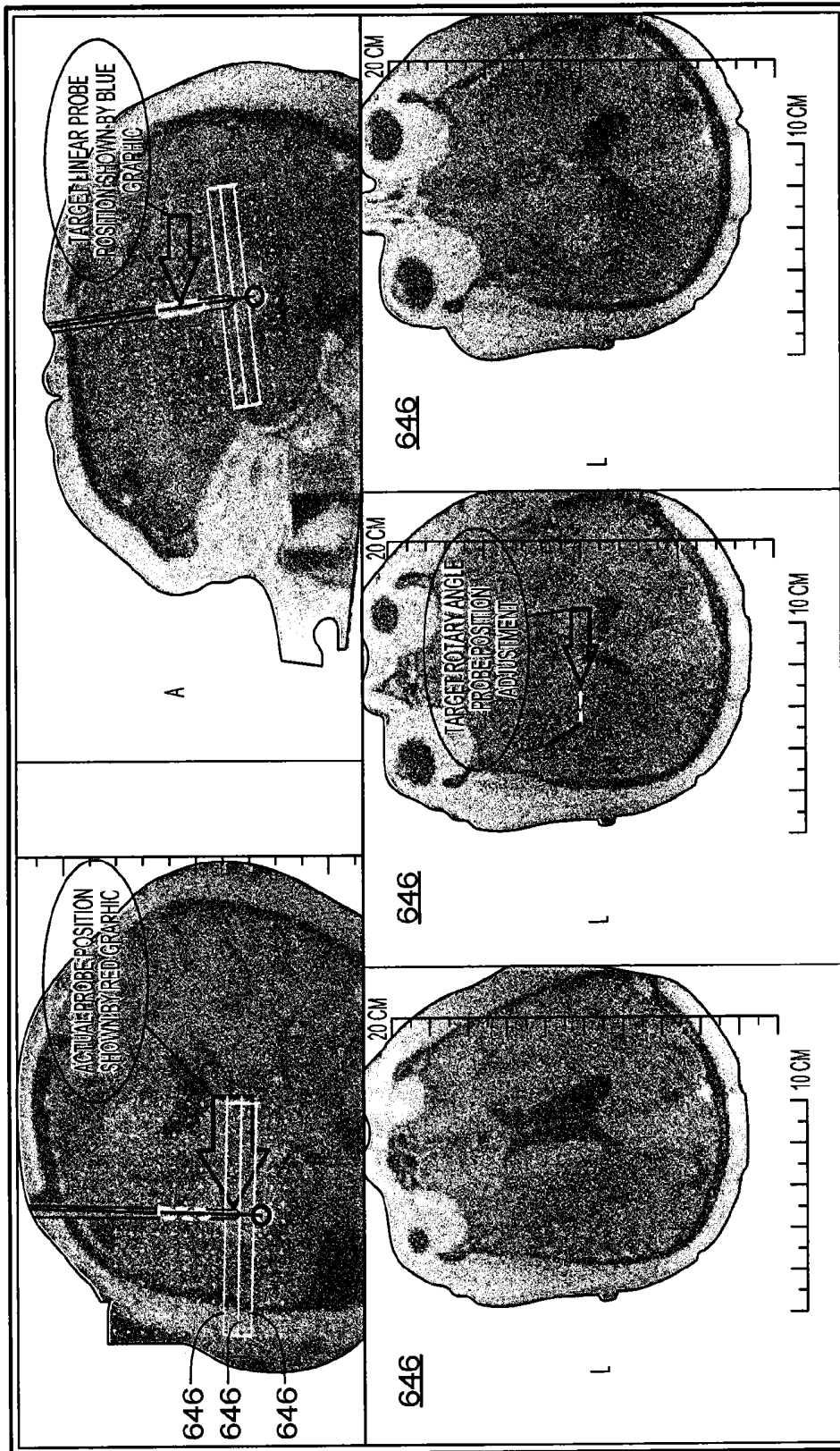


FIG. 96

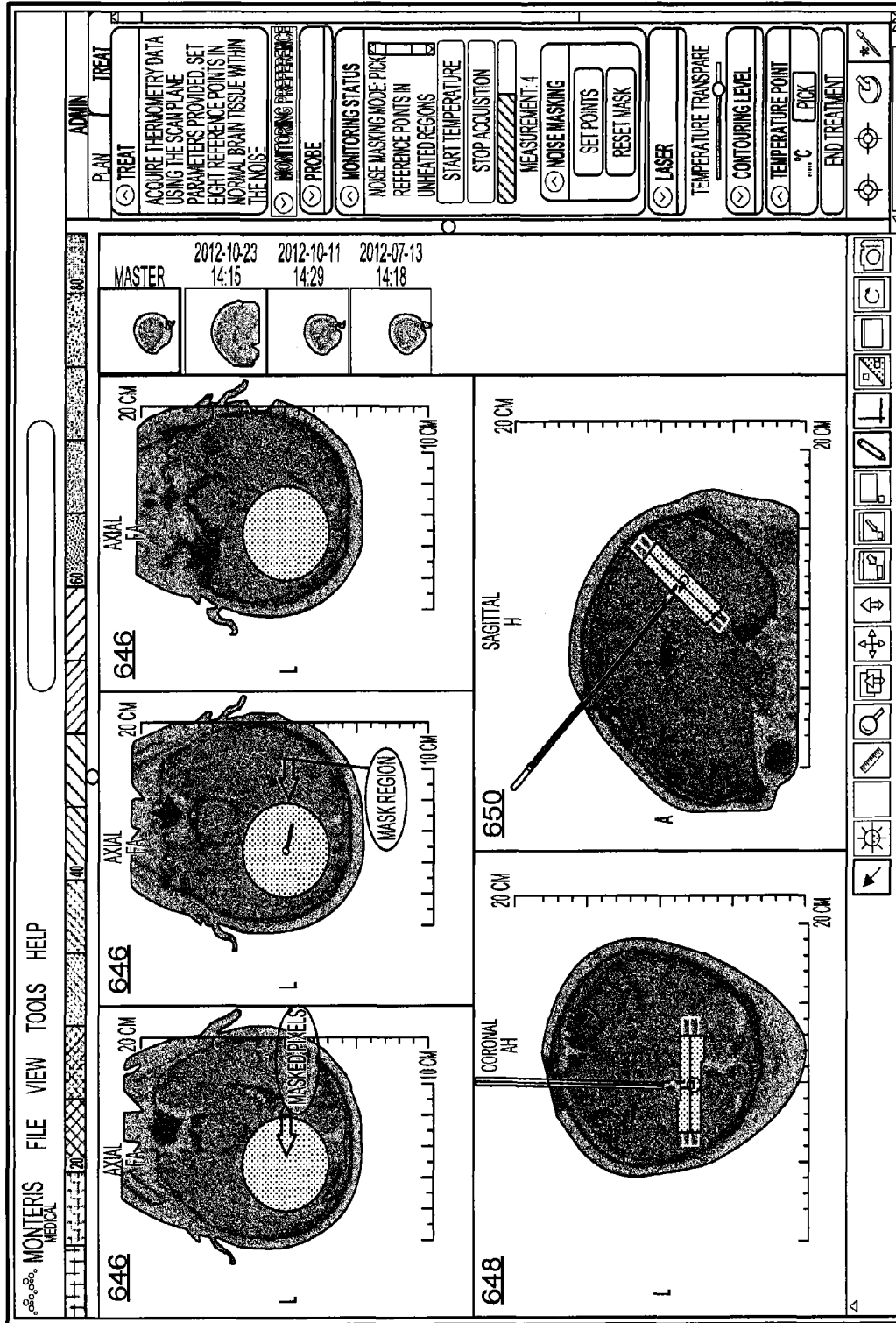


FIG. 97

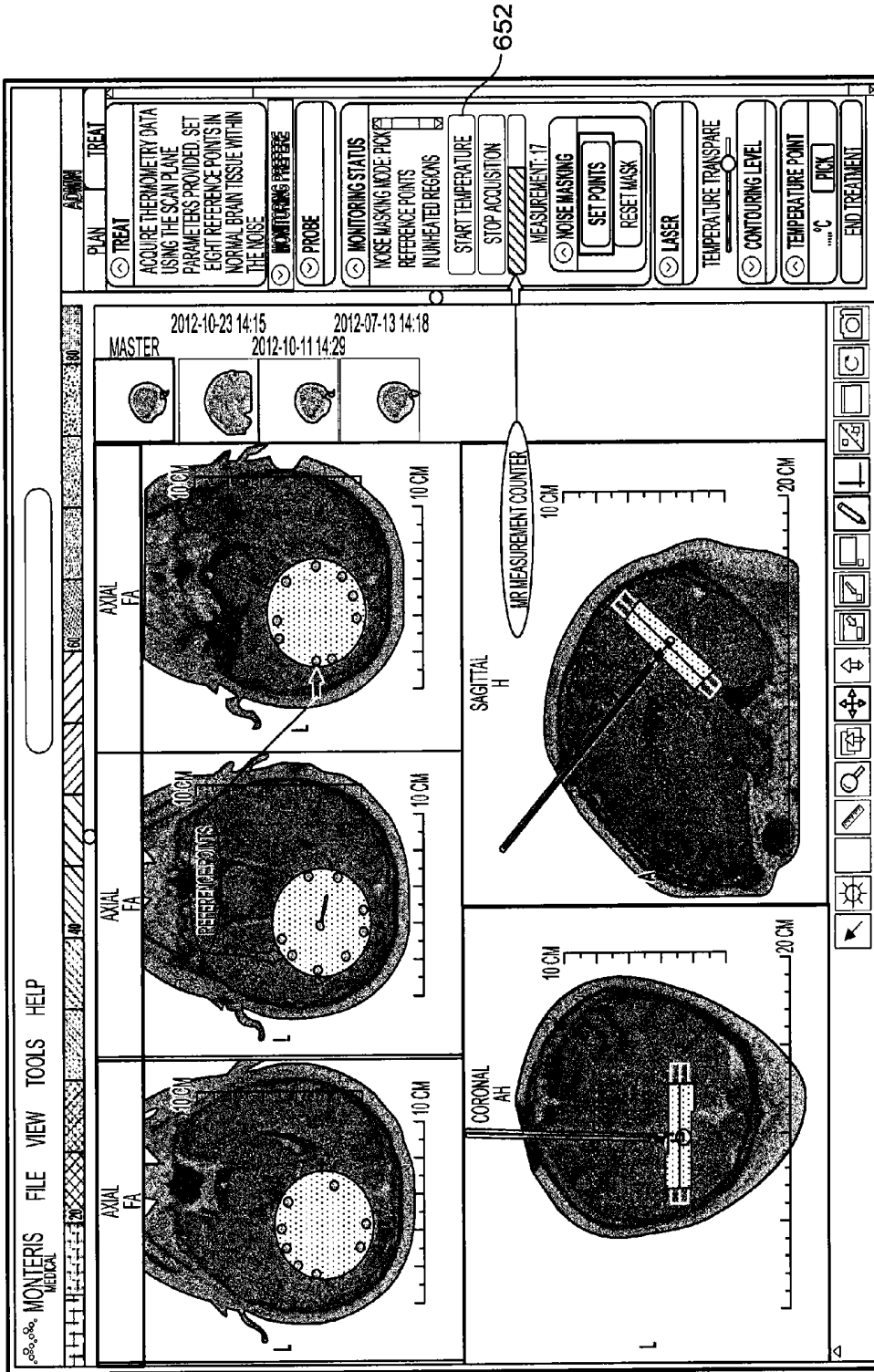


FIG. 98

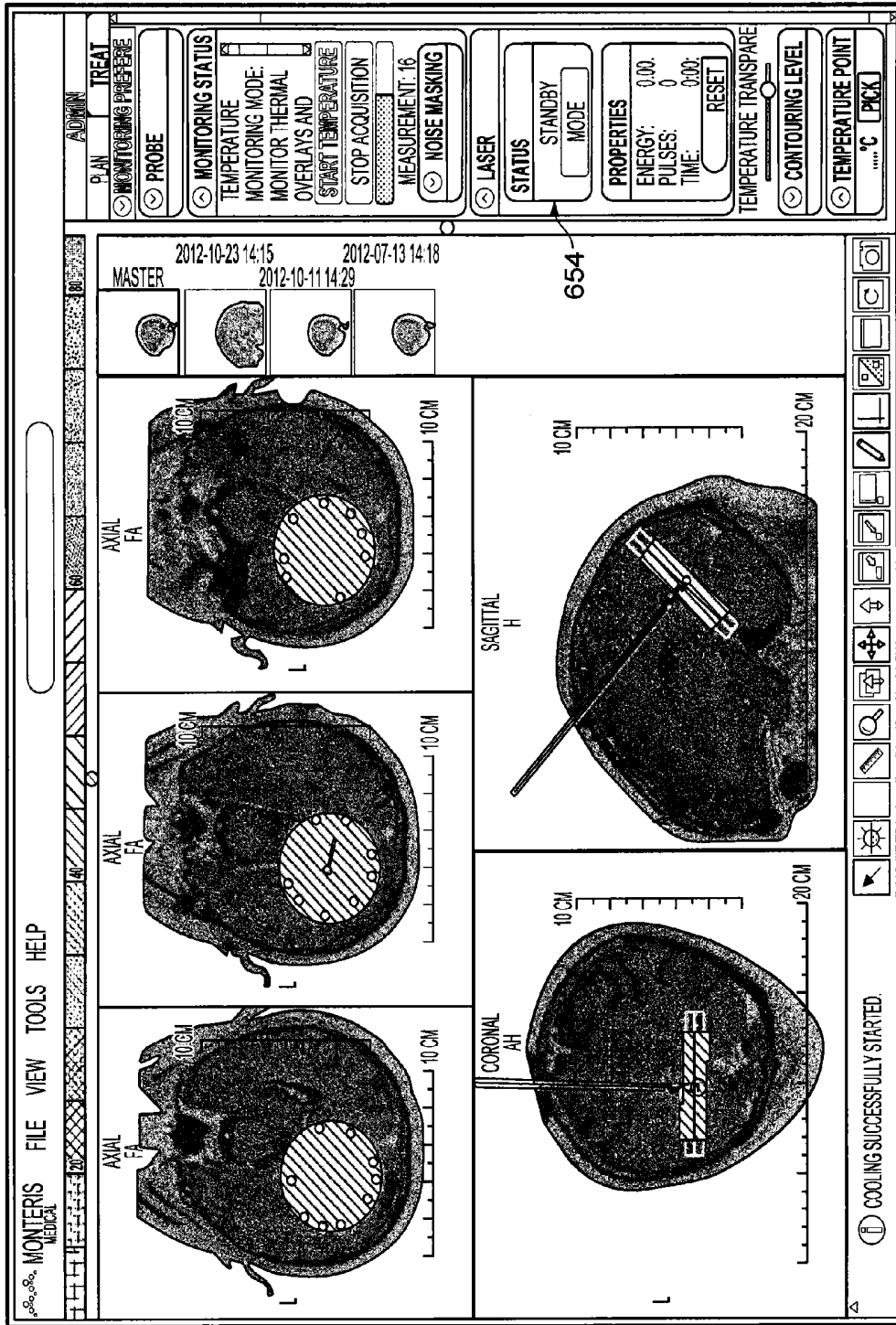


FIG. 99

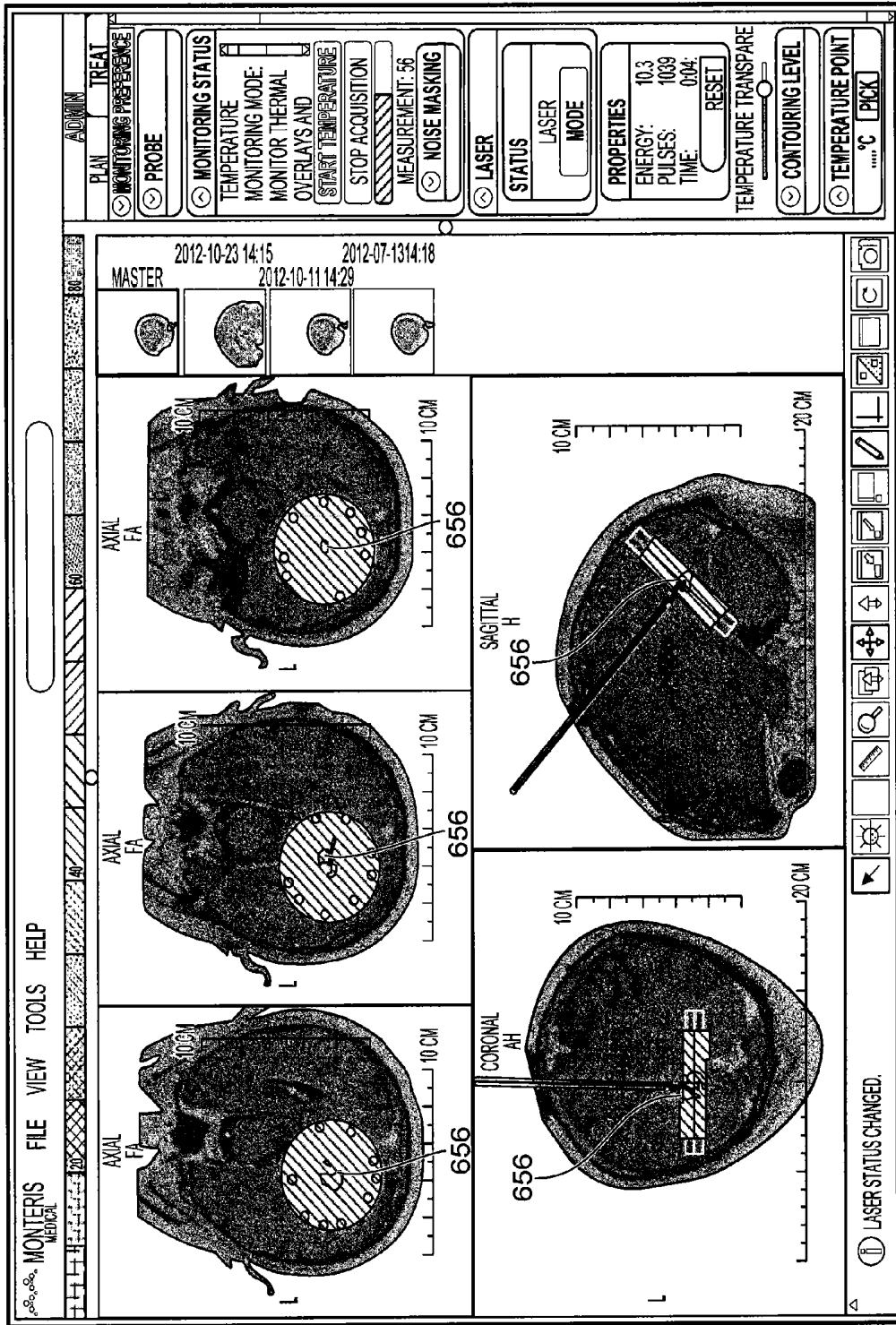


FIG. 100

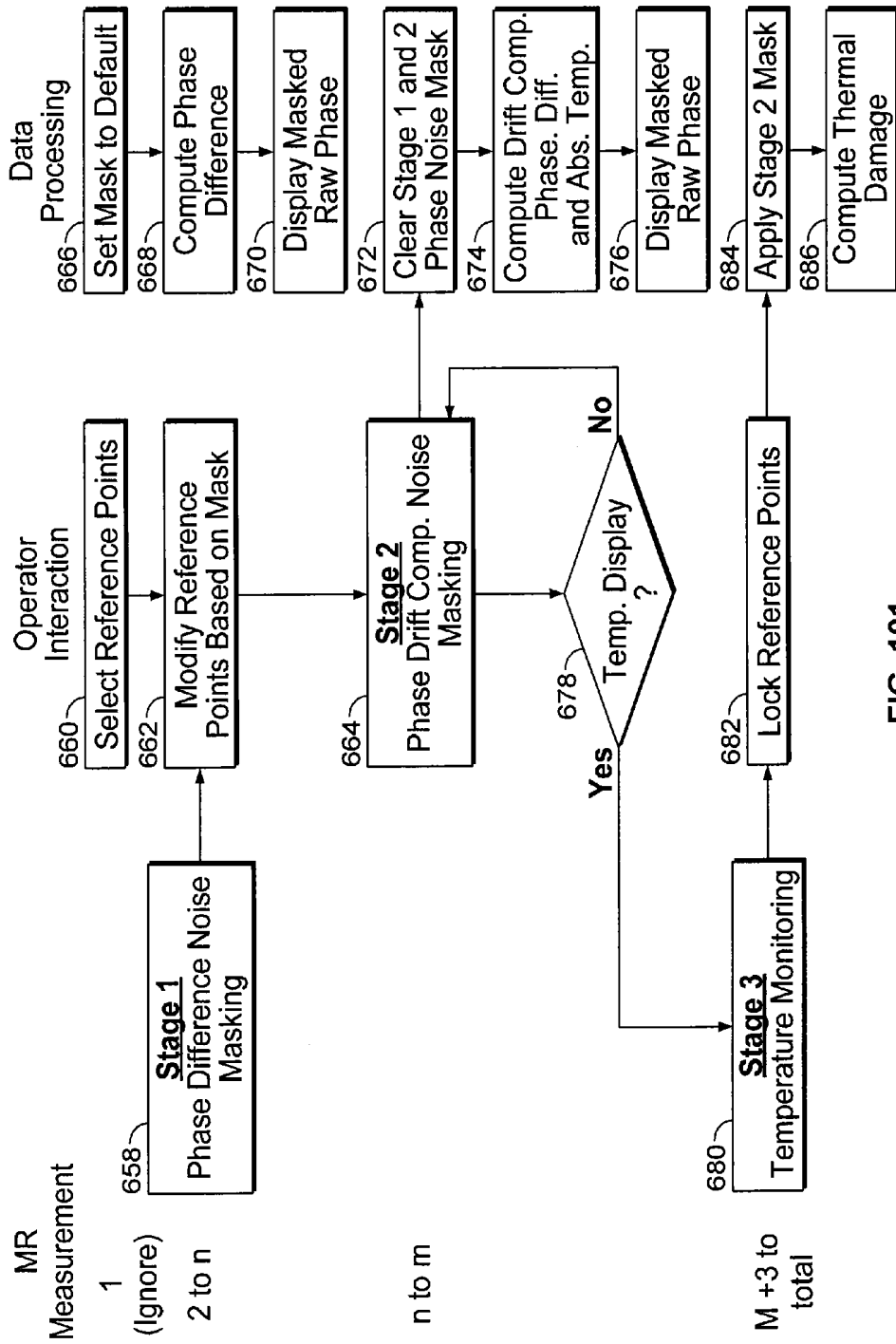


FIG. 101

MONITORING AND NOISE MASKING OF THERMAL THERAPY

CROSS-REFERENCE TO RELATED APPLICATIONS

This application relates to and incorporates by reference the disclosures of: U.S. Ser. No. 12/540,500, filed Aug. 13, 2009, published as U.S. 2010/0042111; U.S. Ser. No. 12/540,558, filed Aug. 13, 2009, published as U.S. 2010/0042112; PCT/IB2012/051716, filed Apr. 5, 2012, published as WO 2012/137179; U.S. Pat. No. 8,256,430, filed Dec. 17, 2007, issued Sep. 4, 2012; U.S. Pat. No. 7,691,100, filed Aug. 25, 2006, issued Apr. 6, 2010; U.S. Pat. No. 7,344,529, filed Nov. 5, 2003, issued Mar. 18, 2008; U.S. Pat. No. 7,167,741, filed Dec. 14, 2001, issued Jan. 23, 2007; and PCT/CA01/00905, filed Jun. 15, 2001, published as WO/2001/095821.

This application is a continuation of U.S. application Ser. No. 13/838,310, filed Mar. 15, 2013, which claims the benefit of U.S. Provisional Application Ser. Nos. 61/728,068, filed Nov. 19, 2012, U.S. 61/664,791, filed Jun. 27, 2012, and U.S. 61/759,197, filed Jan. 31, 2013, the content of each of which is incorporated by reference in its entirety.

BACKGROUND

Approximately 10% of cancerous brain tumors are “primary” tumors, meaning that the tumors originate in the brain. The primary tumors typically consist of brain tissue with mutated DNA that aggressively grows and displaces or replaces normal brain tissue. The most common of the primary tumors are known as gliomas, which indicate cancer of the glial cells of the brain. In most instances, primary tumors appear as single masses. However, these single masses can often be quite large, irregularly-shaped, multi-lobed and/or infiltrated into surrounding brain tissue.

Primary tumors are generally not diagnosed until the patient experiences symptoms, such as headaches, altered behavior, sensory impairment, or the like. However, by the time the symptoms develop the tumor may already be large and aggressive.

One well known treatment for cancerous brain tumors is surgery. Surgery involves a craniotomy (i.e., removal of a portion of the skull), dissection, and total or partial tumor resection. The objectives of surgery include removal or lessening of the number of active malignant cells within the brain, and a reduction in the pain or functional impairment due to the effect of the tumor on adjacent brain structures. However, by its very nature, surgery is highly invasive and risky. Furthermore, for some tumors surgery is often only partially effective. In other tumors, surgery itself may not be feasible. Surgery may risk impairment to the patient, it may not be tolerable by the patient, and/or it may involve significant costs and recovery.

Another well known treatment for cancerous brain tumors is stereotactic radiosurgery (SRS). In particular, SRS is a treatment method by which multiple intersecting beams of radiation are directed at the tumor such that the point of intersection of the beams receives a lethal dose of radiation, while tissue in the path of any single beam remains unharmed. SRS is non-invasive and is typically performed as a single outpatient procedure. However, confirmation that the tumor has been killed or neutralized is often not possible for several months post-treatment. Furthermore, in situations where high doses of radiation may be required to kill a tumor, such as in the case of multiple or recurring tumors, it is common for the

patient to reach the toxic threshold prior to killing all of the tumors, where further radiation is inadvisable.

More recently, the treatment of tumors by heat (also referred to as hyperthermia or thermal therapy) has been developed. In particular, it is known that above 57° C. all living tissue is almost immediately and irreparably damaged and killed through a process called coagulation necrosis or ablation. Malignant tumors, because of their high vascularization and altered DNA, are more susceptible to heat-induced damage than normal tissue. Various types of energy sources may be used, such as laser, microwave, radiofrequency, electric, and ultrasound sources. Depending upon the application and the technology, the heat source may be extracorporeal (i.e., outside the body), extrastitial (i.e., outside the tumor), or interstitial (i.e., inside the tumor).

SUMMARY

One exemplary treatment of a tissue includes interstitial thermal therapy (ITT), which is a process designed to heat and destroy a tumor from within the tumor itself. In this type of therapy, energy may be applied directly to the tumor rather than passing through surrounding normal tissue, and energy deposition can be more likely to be extended throughout the entire tumor.

One exemplary ITT process begins by inserting an optical fiber into the tumor, wherein the tumor has an element at its “inserted” end that may redirect laser light from an exterior source in a direction generally at right angles to the length of the fiber. The energy from the laser may therefore extend into the tissue surrounding the end or tip and effects heating. The energy may be directed in a beam confined to a relatively shallow angle so that, as the fiber is rotated, the beam may also rotate around the axis of the fiber to effect heating of different parts of the tumor at positions around the fiber. The fiber may be moved longitudinally and rotated to effect heating of the tumor over a full volume of the tumor with the intention of heating the tumor to the required temperature. This may be done, in some aspects, without significantly affecting the surrounding tissue. An exemplary fiber used in the ITT process may be controlled and manipulated by a surgeon, in one implementation, with little or no guidance apart from the surgeon’s knowledge of the anatomy of the patient and the location of the tumor. In another implementation, medical images may be used to provide guidance when applying the controlled heating. For example, a location of tumors and other lesions to be excised can be determined using a magnetic resonance imaging system (herein MRI). Utilizing MRI imaging in real time guidance may provide controlled accuracy, while contemporaneous thermography may provide accurate temperature information in determining whether a tissue has been ablated or necrotized.

A system or method for effecting treatment to a tissue can include an automated drive mechanism including a holder to hold a treatment device. The drive mechanism can be coupled to one or more wires or umbilicals such that a translation of the one or more wires or umbilicals effects one or more of a longitudinal displacement of the holder and a rotation of the holder.

The system or method may include a controller that may include an input interface to process position control signals for setting a position of the treatment device, and may further include an output interface to translate the one or more wires based on the position control signals.

The system or method may include a guide mechanism that may be attachable to a surface of a patient. The guide mechanism may include a base structure that may be configured to

remain stationary relative to the patient when the guide mechanism is attached to the surface of the patient in a locked state. The guide mechanism may include a tilt portion that is coupled to the base structure. The tilt portion may be structured so as to hold the drive mechanism at a position that is separated from the surface of the patient. The tilt portion may provide an adjustable tilt between a trajectory of the drive mechanism and the base structure.

The guide mechanism may include a rotation portion that provides an adjustable rotation of the tilt portion relative to the base structure. The drive mechanism may be motorless and consist of thermal imaging compatible components. The drive mechanism may not include an electric motor, and may be included in an MRI or MRI head coil.

The controller may be configured to process a sequence of the position control signals to: move the holder to a first position for effecting the treatment to the tissue at a first portion of the tissue that coincides with the first position; and move the holder to a second position for effecting the treatment to the tissue at a second portion of the tissue that coincides with the second position.

A workstation may be included to transmit the position control signals to the controller and to display thermometry images of the tissue.

The workstation may continuously display the thermometry images of the tissue during the treatment to the tissue at the first and second portions of the tissue, and while the holder moves between the first and second positions.

An energy emission probe may be the treatment device, wherein the probe generates a plurality of different output patterns.

The probe may include a first laser fiber for outputting a symmetrical output pattern with respect to a longitudinal axis of the first laser fiber, and the probe may include a second laser fiber for outputting an asymmetrical output pattern with respect to a longitudinal axis of the second laser fiber.

An energy source may be included to generate energy for the probe. A workstation may be included to transmit the position control signals to the controller, and to transmit energy control signals to the energy source. The workstation may be configured to process a sequence of the energy control signals to: effect a symmetrical treatment to the tissue with the probe; and effect an asymmetrical treatment to the tissue with the probe after the symmetrical treatment.

The system or method may include a laser source to generate laser energy for the laser probe. The workstation may transmit the position control signals to the controller, and may transmit laser control signals to the laser source. The workstation may be configured to process a sequence of the position and laser control signals to: move the holder to a first position for effecting the treatment to the tissue at a first portion of the tissue that coincides with the first position; effect a symmetrical treatment to the first portion of the tissue with the first laser fiber; move the holder to a second position for effecting the treatment to the tissue at a second portion of the tissue that coincides with the second position; and effect an asymmetrical treatment to the second portion of the tissue with the second laser fiber.

The workstation may be configured to display thermometry images of the tissue continuously throughout processing of the sequence of the position and laser control signals and throughout moving the holder and effecting the symmetrical and asymmetrical treatments.

The system or method may include an imaging system to output images of the tissue and the treatment device, including thermometry images of the tissue, in real time, continuously throughout one or more steps of effecting the treatment

to the tissue. The workstation may transmit the position control signals to the controller based on one or more of the images, as the images are received by the workstation in real time, and may display, in real time, one or more of the images throughout the one or more steps of effecting the treatment to the tissue.

The workstation may display, in real time, the thermometry images of the tissue with the images of the tissue and the treatment device continuously throughout a processing of the position control signals and throughout moving the holder and effecting the treatment to the tissue.

The workstation may process, in real time, the images of the tissue and the treatment device and the thermometry images of the tissue to forecast errors or interruptions in the treatment to the tissue and display a corresponding warning.

The system or method may include an energy emission probe as the treatment device. The energy emission probe may include one or more emitters selected from: a laser fiber, a radiofrequency emitter, a high-intensity focused ultrasound emitter, a microwave emitter, a cryogenic cooling device, and a photodynamic therapy light emitter.

The energy emission probe may include a plurality of the emitters, where the plurality of the emitters may be longitudinally spaced with respect to a longitudinal axis of the energy emission probe.

The system or method may include a guide sheath including a plurality of probes of different modalities as the treatment device. The modalities may include one or more of: laser, radiofrequency, high-intensity focused ultrasound, microwave, cryogenic, photodynamic therapy, chemical release and drug release.

The guide sheath may include one or more off-axis holes for positioning an emitting point of one or more of the plurality of probes at an off-axis angle.

The system or method may include one or more processors and circuits that embody portions of aspects of various functions by executing corresponding code, instructions and/or software stored on tangible memories or other storage products. A display may include various flat-panel displays, including liquid crystal displays.

The foregoing general description of the illustrative implementations and the following detailed description thereof are merely exemplary aspects of the teachings of this disclosure, and are not restrictive.

BRIEF DESCRIPTION OF THE DRAWINGS

A more complete appreciation of this disclosure and many of the attendant features thereof will be readily obtained as the same becomes better understood by reference to the following detailed description when considered in connection with the accompanying drawings, wherein:

FIG. 1 is an illustration of exemplary relative locations of an MRI Control Room, an MRI Scan Room, and an MRI Equipment Room;

FIG. 2 is an illustration of a patient inserted into an MRI system;

FIGS. 3-4 illustrate components of an exemplary probe;

FIG. 5 illustrates a probe driver;

FIG. 6 illustrates an interface platform disconnected from a patient platform of a stabilization system;

FIGS. 7A-7B illustrate a connector module being connected/disconnected to an interface platform;

FIG. 8 illustrates a workstation;

FIG. 9 illustrates exemplary hardware of a workstation;

FIG. 10 illustrates a commander/interface platform engagement;

FIG. 11A illustrates a probe follower being aligned with a miniframe;

FIG. 11B illustrates a rotary test tool for a probe follower;

FIG. 12 is an exemplary screen shot of a display of an interface platform;

FIG. 13 illustrates a ruler and depth stop of an exemplary probe;

FIG. 14 is an illustration of a commander/interface platform engagement with a connector module;

FIG. 15 is a photograph of testing an output of a probe;

FIG. 16 illustrates sliding a probe into a probe follower;

FIGS. 17-19 illustrate an exemplary procedure overview including an algorithmic process that outlines portions of a procedure for treating a patient;

FIG. 20 is a perspective view of a portion of a miniframe;

FIG. 21 is a top plan view of a miniframe according to a first rotational position;

FIG. 22 is a top plan view of a miniframe according to a second rotational position;

FIG. 23 is a perspective view of a rotation portion of a miniframe in a locked configuration;

FIG. 24 is a perspective view of a rotation portion of a miniframe in an unlocked configuration;

FIG. 25 is a perspective view of a cam of a miniframe;

FIG. 26 is a perspective view of a frame of a miniframe;

FIG. 27 is a perspective view of a retaining ring of a miniframe;

FIG. 28 is a top perspective view of a central housing of a miniframe;

FIG. 29 is a bottom perspective view of a central housing of a miniframe;

FIGS. 30-31 illustrate an unlocked engagement between a central housing and a cam;

FIGS. 32-33 illustrate a locked engagement between a central housing and a cam;

FIG. 34 is a side profile view of a tilt portion of a miniframe in a first tilt position;

FIG. 35 is a side profile view of a tilt portion of a miniframe in a second tilt position;

FIG. 36 is a perspective view of a tilt portion of a miniframe in a locked configuration;

FIG. 37 is a perspective view of a tilt portion of a miniframe in an unlocked configuration;

FIGS. 38-39 are front and rear top perspective views of a locking arm;

FIGS. 40-41 are top and bottom perspective views of a locking arm and a tilt portion in an unlocked position;

FIGS. 42-43 are top and bottom perspective views of a locking arm and a tilt portion in a locked position;

FIGS. 44-45 are top and bottom perspective views of a tilt portion;

FIG. 46 is perspective view of a foot attached to a leg in an unlocked configuration;

FIG. 47 is perspective view of a foot attached to a leg in a locked configuration;

FIG. 48 is perspective view of a foot;

FIG. 49 is perspective view of a foot attached to a spike plate;

FIG. 50 is perspective view of to a spike plate;

FIG. 51 is perspective view of a spike;

FIGS. 52-54 are, respectively, a bottom perspective view, a top perspective view, and a side view of a foot cap;

FIG. 55 is an illustration of a commander and an interface platform;

FIG. 56 is a schematic illustration of a knob of a commander coupled to a drive mechanism of an interface platform;

FIG. 57 is schematic cross section of a side-fire probe;

FIG. 58 is schematic cross section of a diffuse-tip probe;

FIGS. 59-70 illustrate profiles of exemplary types of probe tips;

FIG. 71A illustrates a schematic cross section of a probe in a guide sheath having an off-axis hole;

FIG. 71B illustrates a schematic cross section of a plurality of probes in a guide sheath having an off-axis hole;

FIG. 72 is a schematic illustration of a probe tip having a plurality of longitudinally space apart energy emitters;

FIG. 73 is a schematic cross section of a side-lire probe and a diffuse tip probe together in a common capsule;

FIG. 74 is a schematic cross section of a capsule attached to a laser fiber;

FIGS. 75-77 illustrate exemplary dimensions of components of an exemplary probe;

FIG. 78 is an illustration of a front perspective view of a patient platform incorporating portions of a head fixation and stabilization system;

FIG. 79 is an illustration of a side perspective view of a patient platform incorporating portions of a head fixation and stabilization system;

FIG. 80 is an illustration of a perspective view of a patient inserted into an MRI, with a head fixation and stabilization system installed;

FIG. 81 is a schematic illustration of a head fixation ring attached to a patient's head;

FIG. 82 is a schematic illustration of one second half of a head coil;

FIG. 83 is a schematic illustration of another second half of a head coil;

FIGS. 84-100 are exemplary screenshots of a graphical user interface of a workstation; and

FIG. 101 is an illustration of an algorithmic sequence for reference point selection, noise masking, and thermal shaping.

DETAILED DESCRIPTION OF THE ILLUSTRATIVE EMBODIMENTS

In the drawings, like reference numerals designate identical or corresponding parts throughout the several views. Further, as used herein, the words "a," "an" and the like generally carry a meaning of "one or more," unless stated otherwise.

Further, in individual drawings figures, the components/features shown are drawn to scale to exemplify a particular implementation. For some drawings, components/features are drawn to scale across separate drawing figures. However, for other drawings, components/features are shown magnified with respect to one or more other drawings. Measurements and ranges described herein relate to exemplary implementations and can identify a value or values within a range of 1%, 2%, 3%, 4%, 5%, or, preferably, 1.5% of the specified value(s) in some implementations.

I. System And Workflow

System

A system in accordance with this disclosure incorporates magnetic resonance imaging (MRI) compatible laser devices and accessories for effective and controlled delivery of thermal therapy to a wide range of locations and tumor sizes within a brain. The system, however, is not limited to MRI-guided thermal therapy, as other therapies such as computer tomography (CT) can also be utilized. Further, this disclosure refers to an MRI scanner as an exemplary medical imaging machine, which may be referred to simply as an MRI.

The system includes an interface platform (herein an interface platform or interface console), a system electronics rack

and components (herein rack), a control workstation (herein workstation), a probe driver, and a probe. The system can also include a stereotactic miniframe, a head coil and stabilization system (herein stabilization system), an instrument adaptor, and an MRI trajectory wand. All of the above components are MRI compatible, which refers to a capability or limited capability of a component to be used in an MRI environment. For example, an MRI compatible component operates and does not create significant interference with MRI in exemplary magnetic flux densities of 1.5 T or 3.0 T, where no hazards are known for a specified environment (e.g., 1.5 T or 3.0 T). Compatibility can also be defined with respect to other magnetic flux densities, including 0.5 T, 0.75 T, 1.0 T, 2 T or 5 T. "MRI Safe" refers to an item that poses no known hazards in all MR environments. "MRI Unsafe" refers to an item that is not MRI compatible and is known to pose a hazard in MR environments. This equipment should not be taken into the MRI room within a 5 Gauss perimeter line.

The interface platform attaches to an MRI patient table and provides supporting electronics for the probe driver and interconnections for the probe. The system electronics rack includes necessary cables, penetration panels and small hardware for system mechanical, electrical, and electronic operation. The workstation includes a user interface, e.g., a graphical user interface (GUI), for procedure planning, interactive monitoring of procedures, and interfaces to the MRI and hardware subsystems. The probe driver allows for precise positioning, stabilization and manipulation of a probe. The probe can be a gas-cooled probe for delivering controlled energy to a tissue. As discussed in Section IV, the length and diameter of the probe can be pre-selected and varied.

The stereotactic miniframe includes at least a portion that is MRI visible and used for trajectory determination, alignment, and guidance of the probe. The stabilization system is a head fixation device to immobilize a patient's head. The instrument adaptor can include a set of three reducing tubes of, e.g., 1.9 ± 0.2 mm, 2.2 ± 0.2 mm and 2.6 ± 0.2 mm, that guide neurosurgical devices such as a biopsy needle through the stereotactic miniframe. The MRI trajectory wand is an MRI visible, fluid-filled tube which is placed into the stereotactic miniframe to allow trajectory confirmation of intended alignment to the target via MRI.

Exemplary MRI systems that can be utilized together with the features discussed herein include those manufactured by Siemens AG, Munich, Germany (including the MAGNETOM AVANTO, TRIO, ESPREE, VERIO MRI Systems, which are trademarks and/or trade names of Siemens AG). Further, exemplary MRI systems include those manufactured by General Electric Company, Fairfield, Conn. (including the SIGNA, OPTIMA and DISCOVERY MRI systems, which are trademarks and/or trade names of General Electric Company).

FIG. 1 illustrates an exemplary layout of various MRI components, including the MRI system in an MRI scan room, a control workstation in an MRI control room, and an electronics rack in an MRI equipment room. Also shown in FIG. 1 is an interface platform secured to a patient table of the MRI system.

FIG. 2 illustrates an exemplary layout of a patient on a patient table of an MRI system. An interface platform is secured to the patient table together with a head coil and stabilization system. A probe and probe driver are coupled to a stereotactic miniframe, and to the interface platform via umbilicals. A cable provides data, laser, fluid, etc. connections between these components and the electronics rack in the MRI equipment room.

The probe can be a laser delivery probe that is used to deliver laser interstitial thermal therapy. The probe is preferably composed of MR compatible materials allowing for simultaneous laser application and thermal imaging, and can be provided in multiple lengths and dimensions. FIGS. 3 and 4 illustrate exemplary aspects of a laser probe. Other types of probes that can be utilized with the components and procedures discussed herein include radiofrequency (RF), high-intensity focused ultrasound (HiFu), microwave, cryogenic, chemical release, which may include photodynamic therapy (PDT), and drug releasing probes. For example, modalities of probes other than a laser energy modality can be utilized. Treatments in accordance with the descriptions provided in this disclosure include treatments that ablate (i.e., "treat") a tissue to destroy, inhibit and/or stop one or more or all biological functions of the tissue. Ablation agents include, but are not limited to, laser, RF, HiFu, microwave, cryogenic, PDT and drug or chemical release. A corresponding probe and/or an other instrument, such as a needle, fiber or intravenous line can be utilized to effect treatment by one or more of these ablation agents.

A probe tip is shown in FIG. 3, which indicates an insertion end. A probe interface/depth stop adjustment provides an interface for cabling, as well as for alignment with the probe driver and/or the stereotactic miniframe. An end opposite the insertion end includes probe connectors for energy delivery, cooling, etc. FIG. 4 is an enlarged view of the probe interface to probe tip portion of the probe shown in FIG. 3.

FIG. 5 illustrates a probe driver, which generally includes a commander, umbilicals, a follower, and a position feedback plug that receives position feedback signals from potentiometers within the follower. A probe can be inserted into the follower, and the follower can control a rotational and longitudinal alignment of the probe.

The probe driver is mounted to the interface platform, as shown for example in FIG. 2. A position feedback plug connects to the interface platform in order to communicate the probe's position to the system. The probe driver is used to rotate or translate (extended or retract) the probe. The probe driver in this illustrated implementation can provide, at a minimum, a translation of 20-80 mm, 30-70 mm, 40-60 mm or 40 mm, with a maximum translation of 60 mm, 80 mm, 100 mm, 120 mm or 60-150 mm. The probe driver in this illustrated implementation can also provide, at a minimum, a rotation of 300°-340°, with a maximum rotation of 350°, 359°, 360°, 540°, 720° or angles therebetween. The probe driver is comprised of the commander and the follower connected by an umbilical cable (umbilicals). Included with the probe driver can be a rotary test tool that can be used during a self-test procedure to simulate an attachment of a probe to the follower.

FIG. 6 illustrates a coupling between an interface platform and a head end of a stabilization system. An attachment of the interface platform to the head end of the stabilization system can be performed by sliding two interface platform arms into two corresponding receptacles of the stabilization system.

FIGS. 7a-7b illustrate an interface platform connector module of interface platform, which is detachably connected to the interface platform by a locking mechanism. This module is capable of accepting probe extension lines/cables. The connector module can be locked in place by twisting the connector module lock 80-100° or 90° counterclockwise.

FIG. 8 illustrates an exemplary workstation situated in the MRI control room. The workstation can include an emergency stop (E-Stop) switch, which includes a red light to indicate that it is on (i.e., the presence of the red light indicates the system and/or the MRI system has been stopped via the

emergency stop switch). To release the switch, the emergency stop switch can be twisted clockwise. The workstation can also include a power switch at the side of a monitor.

FIG. 9 illustrates an exemplary processing system, and illustrates exemplary hardware found in a controller or computing system (such as a personal computer, i.e., a laptop or desktop computer, which can embody a workstation according to this disclosure) for implementing and/or executing the processes, algorithms and/or methods described in this disclosure. A processing system in accordance with this disclosure can be implemented in one or more the components shown in FIG. 1. One or more processing systems can be provided to collectively and/or cooperatively implement the processes and algorithms discussed herein.

As shown in FIG. 9, a processing system in accordance with this disclosure can be implemented using a microprocessor or its equivalent, such as a central processing unit (CPU) and/or at least one application specific processor ASP (not shown). The microprocessor is a circuit that utilizes a computer readable storage medium, such as a memory circuit (e.g., ROM, EPROM, EEPROM, flash memory, static memory, DRAM, SDRAM, and their equivalents), configured to control the microprocessor to perform and/or control the processes and systems of this disclosure. Other storage mediums can be controlled via a controller, such as a disk controller, which can controls a hard disk drive or optical disk drive.

The microprocessor or aspects thereof, in alternate implementations, can include or exclusively include a logic device for augmenting or fully implementing this disclosure. Such a logic device includes, but is not limited to, an application-specific integrated circuit (ASIC), a field programmable gate array (FPGA), a generic-array of logic (GAL), and their equivalents. The microprocessor can be a separate device or a single processing mechanism. Further, this disclosure can benefit from parallel processing capabilities of a multi-cored CPU.

In another aspect, results of processing in accordance with this disclosure can be displayed via a display controller to a monitor. The display controller preferably includes at least one graphic processing unit, which can be provided by a plurality of graphics processing cores, for improved computational efficiency. Additionally, an I/O (input/output) interface is provided for inputting signals and/or data from microphones, speakers, cameras, a mouse, a keyboard, a touch-based display or pad interface, etc., which can be connected to the I/O interface as a peripheral. For example, a keyboard or a pointing device for controlling parameters of the various processes and algorithms of this disclosure can be connected to the I/O interface to provide additional functionality and configuration options, or control display characteristics. Moreover, the monitor can be provided with a touch-sensitive interface for providing a command/instruction interface.

The above-noted components can be coupled to a network, such as the Internet or a local intranet, via a network interface for the transmission or reception of data, including controllable parameters. A central BUS is provided to connect the above hardware components together and provides at least one path for digital communication there between.

The workstation shown in FIG. 8 can be implemented using one or more processing systems in accordance with that shown in FIG. 9. Further, one or more processors can be utilized to implement any functions and/or algorithms described herein, unless explicitly stated otherwise. Also, the equipment rack and the interface platform each include hardware similar to that shown in FIG. 9, with appropriate changes to control specific hardware thereof.

In some aspects, the workstation outputs signals to the MRI system to actuate particular imaging tasks or to an intermediary system that causes the MRI system to actuate particular imaging tasks. Further, in some aspects, the workstation outputs signals to the electronics rack. The electronics rack includes various actuators and controllers for controlling, e.g., a cooling fluid pressure and a flow rate of the cooling fluid, and a power source that outputs ablative energy. In utilizing a laser probe, the power source is a laser source that outputs light via an optical fiber. As illustrated in FIG. 1, the electronics rack is located in the MRI Equipment Room and includes storage tanks to hold the cooling fluid, one or more inputs to receive signals from the control workstation and/or a separate MRI workstation, a laser generating device, and an output section. The output section includes data and laser output cables that are routed to corresponding components in the MRI Scan Room through an appropriate portal to minimize interface with or by the MRI system. As discussed in other portions of this disclosure, the cables are connected at or by the interface platform to corresponding components to effect and actuate control of the components.

FIG. 10 illustrates the connecting of a commander to an interface platform, and the attachment of a position feedback line and probe lines to the interface platform and/or the connector module thereof. In these drawings "IP" refers to the interface platform. The commander includes holes for mounting posts of the interface platform body, and a latch of the interface platform engages the commander when the commander is properly inserted. Consistent with the descriptions provided in Section III, the commander includes knobs or dials that are coupled to a drive system of the IP. Command signals to actuate the drive system from, e.g., the workstation, are transmitted or routed to the IP, causing the drive system to operate one or both of the knobs or dials to effect movement of a probe or other member attached to the probe driver follower in accordance with the disclosures provided herein.

FIGS. 11a and 11b illustrate a coupling between the follower, which includes directional interface tabs 1 and 2, and a stereotactic miniframe, which includes directional interface notches 1 and 2, to ensure a proper registered alignment between the follower and the stereotactic miniframe. The miniframe also includes a directional interface locking thumbscrew to secure the follower to the miniframe. FIG. 11b illustrates the attachment of a rotary test tool to the follower to provide position feedback for a probe driver self-test procedure.

This self-test procedure can be executed via software that is displayed/illustrated to a user via the workstation and/or via the interface platform. After attaching the commander of the probe driver to the interface platform and the stereotactic miniframe, directional control and commands from the commander, the interface platform, and/or the workstation can be verified with the rotary test tool.

For installation of the above components, the follower should be kept sterile and manipulated by a sterile person, while the commander can be passed to a non-sterile person. The non-sterile person attaches the commander to the interface platform and engages the latch to lock the commander in place by twisting the latch to the centered position, as shown in FIG. 10. FIG. 10 further illustrates the attachment of a position feedback line and probe lines to the interface platform and/or the connector module thereof. In these drawings "IP" refers to the interface platform. The commander includes holes for mounting posts of the interface platform body, and a latch of the interface platform engages the commander when the commander is properly inserted.

As illustrated in FIG. 11a, the sterile person slides the sterile follower into the directional interface of the miniframe until the directional interface tabs are oriented and fully seated. The follower is then locked in place with the directional interface thumbscrew. Care should be exercised when attaching the follower to the miniframe to prevent unintended trajectory deviation. This could lead to severe injury or death of the patient. Additionally, the position feedback plug (cable) should be connected as shown in FIG. 10, and care should be taken to ensure that the cable for the plug does not rest on the patient during imaging.

The following are warnings, cautions and/or issues that apply to the system described herein.

The system is indicated for use to ablate, necrotize, and/or coagulate soft tissue through interstitial irradiation or thermal therapy in medicine and surgery in the discipline of neurosurgery with 1064 nm lasers, when a thermal probe is utilized in the system. Lasers of other outputs can be utilized, including lasers having wavelengths of 0.1 nm to 1 mm, and lasers in one or more of the ultraviolet, visible, near-infrared, mid-infrared, and far-infrared spectrums. Types of exemplary lasers include gas lasers, chemical lasers, dye lasers, metal-vapor lasers, solid-state lasers, semiconductor lasers, and free electron lasers. In one implementation, one or more wavelengths of the laser is within the visible spectrum, and one or more wavelengths of the laser is within the near-infrared spectrum. The system can be utilized for planning and monitoring thermal therapies under MRI visualization, and can provide MRI-based trajectory planning assistance for the stereotactic placement of an MRI compatible (conditional) probe. It also provides real-time thermographic analysis of selected MRI images.

When interpreted by a trained physician, this system provides information that may be useful in the determination or assessment of thermal therapy. Patient management decisions should not be made solely on the basis of an image analysis.

Probe or laser delivery in highly vascular regions can result in hemorrhage and/or post treatment aneurysm. Probe trajectories which transect or overdosing with thermal energy in regions containing cortical-spinal pathways can result in patient injury and permanent neurological deficits. Protracted surgical sessions with the patient immobilized can result in deep vein thrombosis.

The system should be operated by trained personnel under the direct supervision of a trained physician. Laser eye protection should be worn in the MRI scanner room during operation of a laser. The color perception abilities of an operator should be considered during temperature monitoring in implementations that utilize color maps, where the monitoring is manually performed by the operator. Operators who are color blind or have impaired color perception may not be able to monitor temperature during the procedure which could result in patient injury or death. Only approved accessories should be used. Failure to do so may result in improper performance and/or damage to the equipment with potential to cause harm.

Only approved and verified MRI sequences for thermal imaging should be used in conjunction with this equipment. Failure to do so may result in improper thermal monitoring which could lead to patient injury.

All loaded image data should contain correct patient identification and image orientation markers prior to the commencement of a procedure to ensure an unintended area of the brain is not targeted for thermal delivery which can lead to patient injury.

Extreme care should be taken when determining patient baseline core body temperature by using an MRI compatible

patient monitoring system using an internally placed temperature monitoring probe. Failure to determine an accurate value will result in improper performance of temperature monitoring software with the potential to cause patient injury. During a procedure, the treated tissue should be allowed to return to ambient temperature levels before acquiring subsequent MR thermal imaging.

The system may be contraindicated for patients with certain metallic, electronic or mechanical implants, devices or objects that should not enter the MRI scan room or serious injury may result.

Further, the user should beware of the strong magnetic field in the MRI room. Extreme caution should be used before bringing in any equipment into the MR environment. Only items identified as MR Safe or Compatible/Conditional for the particular environment should be brought into the MR room. No items identified as MR Unsafe should be brought into the MR suite within the 5 Gauss line. Serious injury can result if any equipment which is MR unsafe is brought into the MRI suite.

The following are specific warnings that apply to the probe driver and the probe.

These components are intended for single use, and should not be reused, reprocessed or re-sterilized. Reuse, reprocessing or re-sterilization can compromise the structural integrity of the device and/or lead to device failure which in turn may result in patient injury, illness or death. Reuse, reprocessing or re-sterilization may also create a risk of contamination of the device and/or cause patient infection or cross-infection, including, but not limited to, the transmission of infectious disease(s) from one patient to another. Further, contamination of the device may lead to injury, illness or death of the patient.

When aligning and connecting the probe driver follower, the user should confirm that the position displayed on the interface platform is correct. Failure to do so may cause the laser energy delivery direction to be determined incorrectly, potentially resulting in patient harm.

All cables and umbilical in the vicinity of the MRI bore should not form loops as this may result in heating (with the potential to cause burns to the patient) and RF interference (which would affect equipment performance). The probe should be fully engaged to the probe driver prior to manipulating the probe in tissue. The laser in the probe should not be fired if the probe is not inserted in tissue or before the probe connections are made. A desired probe trajectory should be ensured to not interfere with the MR bore or other required equipment prior to the insertion of the probe into tissue.

The probe can be classified as a class 4 laser product in accordance with EN60825-1:2003. Irreversible injury can occur. Laser radiation should not be directed to the retina of the eye. Skin or the eye should not be subjected to direct or reflected laser radiation. Each person inside the laser area should wear protective eyewear.

Laser fiber connections should be made correctly as improper connections can lead to fire danger or operator injury. Laser connections should be fully seated. Failure to do so can cause the receptacle to heat, reduce thermal energy deposition, cause equipment damage or operator or patient injury.

The laser area can be defined by the Nominal Ocular Hazard Distance (NOHD) as 2.8 m from the laser output at the probe tip (when connected) or the extension fiber output on the interface platform. Outside of this region, laser safety eyewear is not required.

An exemplary probe and probe driver can be used under the following conditions: static magnetic field of 1.0, 1.5, 2.0, 2.5, 3.0 or 3.5 Tesla; and spatial Gradient field of 500, 360,

300 or 240 Gauss/cm or less. The whole-body-averaged specific absorption rate (SAR) should not exceed 4, 3, 2, 1.5 or 1 W/kg. Whole body transmitting coils can be used. Local transmitting coils should not be used, but local receiving coils can be used.

MRI image quality may not be affected while the interface platform display is OFF. However, image quality can be affected if the interface platform display is powered ON during acquisition, potentially causing image artifacts.

The probe and probe driver should be inspected carefully prior to use for any breach of the sterile barrier or damage to the contents, and should not be used if the sterile barrier integrity is compromised or the contents damaged.

General preferred operating conditions of the system include: temperature: 15° C. (59° F.) to 30° C. (86° F.) or around 23-26° C.; and relative humidity: <50, 60 or 70%. General preferred storage conditions of the system include: temperature: 10° C. (50° F.) to 40° C. (104° F.); relative humidity: <60%; and keep out of direct sunlight.

The system can use medical grade CO₂ gas as a coolant for a laser probe. Medical grade CO₂ size "E" tanks, unless otherwise labeled, are MR Unsafe and should not be brought into the MR suite within the 5 Gauss line. The electronics rack can be designed to hold two "E" size tanks. For a particular implementation, pressure gauges for each tank should read >4500 kPa (>650 psi) for use. Exemplary pressures of the gas include 600-650, 650-700, 700-750, 750-800, 800-850 and 700-900 psi.

Procedure Workflow

A procedure includes, generally, identifying a tissue in a patient to be treated, planning one or more trajectories for treating the tissue, preparing the patient and components for the treatment, and performing the treatment. Aspects of the various parts of the treatment are described throughout this disclosure, and a particular sequence of treatment steps is described herein.

In pre-planning of a treatment of a patient, pre-treatment DICOM image data is loaded and co-registered via the workstation. An intended treatment region of interest(s) (ROI)(s) and initial trajectory(s) are created and established as desired.

A head coil and fixation system is attached to the patient, which includes positioning the head coil and stabilization system on the surgical table. The patient is immobilized using a head fixation ring. The patient head should be secured with a head fixation device and remain fixed within magnet space for entire imaging portion of the outlined workflow. If the patient head position changes relative to the head fixation device at any point during the procedure, then new imaging should be acquired and co-registered as a master series or thermal energy may be delivered in an unintended area causing patient injury.

A probe entry location into the skull is identified, and a burr hole may be created prior to miniframe attachment or a twist-drill hole should be created following stereotactic miniframe trajectory alignment. The twist-drill hole can have a size of 1-5 mm, 2 mm, 3 mm, 4 mm or 4.5 mm. The stereotactic miniframe is attached to the patient's head, and the miniframe is aligned along the intended trajectory using image-guided navigation. The head coil and fixation system is then attached.

Depending on a site specific workflow, the interface platform may be attached prior to or after MRI trajectory confirmation. The order of these steps is typically determined with the MRI or surgical support team during on-site training. The interface platform is attached to the head end of the head coil and stabilization system, as shown in FIG. 6. Then, the IP power and motor plugs are connected, as shown in FIG. 10.

Trajectory confirmation and beam fiducial marker detection is then performed. The established trajectory of the miniframe should be evaluated using MRI prior to inserting a probe into the brain. Volumetric imaging is recommended to include the entire head and full extent of the miniframe. These images will also visualize a beam fiducial marker located in a portion of the miniframe. This marker is identified to orient the software to the physical direction of the probe. This image data can also be used for treatment planning if pre-treatment image data is not available.

The patient is positioned in the MRI, and MRI imaging is performed to confirm trajectory with an MRI trajectory wand inserted into the miniframe.

Using the workstation within a so-called "Plan Register" workflow step, acquired image data is loaded and co-registered with already loaded pre-planning image data (if any). Using the workstation within a so-called "Plan Volumes" workflow step of the workstation, treatment ROI(s) are defined, if not already defined. Using the workstation within a so-called "Plan Trajectories" workflow step, a rendered probe trajectory(s) along the imaged position of the MRI trajectory wand is established and/or adjusted. Using the workstation within a Treat Align and Auto-Detector step, the fiducial marker of the mini frame is identified/registered and set.

The follower is attached to the miniframe, and the rotary test tool is attached to the follower to provide position feedback for a probe drive self-test step, which confirms that inputs to the follower, via the commander, accurately drive the rotary test tool. Once successful, the rotary test tool is removed by depressing a release button on its side and pulling it back off of the follower. See FIG. 11b. Upon removal of test tool, the rotary position will no longer be valid and will be displayed on the interface platform as "Unset" until the probe is placed into position.

An appropriate probe size is selected, and a corresponding probe is removed from its sterile pouch and placed in the sterile field.

The following steps are taken to set and lock a probe depth stop. The workstation calculates the required length of the probe based on trajectory planning and the intended target. The interface platform displays the probe size for the user in two ways during a system self-test, as shown in FIG. 12, which includes an image of a display screen of the interface platform. FIG. 12 illustrates a required probe size and depth stop setting.

FIG. 13 illustrates adjustment and setting of a depth stop. A first step is to ensure a probe is fully inserted into the ruler/protective cover, as shown in FIG. 13. An audible click should be heard if reinserting the cover into the probe locking interface. The locking interface is then slid so that the probe tip aligns with the required distance measurement on the ruler. Locking buttons at the wider end are then squeezed to lock the depth stop, as shown in FIG. 13. An audible click should be heard when locked. A tapered part/end of both buttons can be squeezed to unlock the depth stop lock.

The proper depth of the probe can be rechecked by matching the probe tip to ruler graduations. Further, it should be rechecked that the depth stop is locked prior to inserting the probe into the brain. An improperly set depth stop can allow the probe tip to be delivered short of or deeper than intended/planned, which may lead to patient injury. The ruler is then removed by depressing the release button shown in FIG. 13.

FIG. 14 illustrates the location of probe connections on the interface platform. Preferably, the sterile person will hand off the probe connector plugs to a non-sterile person to insert the plugs to the associated receptacles on interface platform. The

cooling plug is inserted into the mating receptacle (labeled CO₂). It should click and lock when fully inserted. The arrow on the thermocouple plug should be aligned with the arrow on the receptacle marked THERMOCOUPLE. The plug should be inserted into the receptacle until it clicks and locks. The laser plug should be inserted into the mating receptacle (labeled LASER). Two clicks should be heard; one at half insertion and one at full insertion. With medium force, the connector should be pulled back to ensure it is fully seated and does not pull out. The three connector lines in the connector line bracket should be retained as shown in FIG. 14 to ensure that the lines remain fixed to the interface platform if the specific site that the workflow so requires.

The laser probe laser fiber connector should be completely engaged into the corresponding interface platform receptacle. Failure to do so can cause receptacle heating and reduce the energy delivered to the target tissue. This may result in fire or injury of the user or patient.

The three probe connector lines should be retained in the probe connector line bracket to ensure potential force during disconnection of the probe connectors is not transferred to the probe after insertion into the brain. Force applied to the probe after insertion into the brain can lead to patient injury or death.

The laser is physically interlocked by the workstation until the appropriate workflow step has been reached. The laser interlocks should remain disabled throughout the workflow until treatment monitoring begins. However, the visible pilot laser beam can be enabled. The visible pilot laser can be a class 2 laser product according to IEC 60825-1 having a maximum power of 1 mW. Other maximum powers include 0.5, 0.6, 0.7, 0.8, 0.9, 1.5 and 2-5 mW. The laser should not emit energy when a foot pedal is pressed during a self test. A bright, red laser light should be visible exiting the probe tip in the correct orientation from the probe. Aiming the beam at a surgical glove should produce a bright, red spot, as shown in FIG. 15. If the physician or a user does not see a strong, visible red aiming laser beam exiting the probe tip, then the full insertion of the probe laser plug should be ensured. Otherwise, the probe should be disconnected, and a second probe of the same size should be selected and registered as the first probe was.

When the beam test is successful, a next button can be depressed on the interface platform display to continue the workflow steps shown on the interface platform display. A gas cooling test can then begin. The Next button can be depressed when it has completed.

The tip of the probe can then be inserted into the probe driver follower and into the brain until the probe locking interface comes in contact with a mating adapter on the follower. See FIG. 16. While gently pressing the probe toward the follower, the probe can be twisted until it fully locks onto the follower. An audible click should be heard when the probe is locked into position. This can be confirmed by gently pulling back on the probe to ensure it is properly locked in place, which is shown in FIG. 16.

MRI imaging is performed to confirm delivery of the probe along the intended trajectory. Acquired image data with already loaded pre-planning image data (if any) can be loaded using a Treat Insert workflow step of the workstation. The rendered probe in the workstation can then be adjusted as needed to match the probe artifact on the acquired image. Once the software rendered probe matches the probe artifact on the screen, "Yes" or "Confirm" can be selected through the workstation to confirm trajectory.

In advance of each procedure, a data transfer interface should be enabled following patient registration on the MRI system. If the patient head position changes relative to the

head fixation device at any point during the procedure the user should either register the patient in the MRI system as a new exam or use the MRI positioning lights to "re-landmark" the patient into magnet space center position. The entire head should be re-scanned to include the miniframe using a 3D volumetric scan. This scan should be co-registered with all other loaded planning sequences and be set as the master or thermal dose may be delivered in an unintended area causing patient injury.

Using the workstation, the rendered probe's trajectory can be adjusted to the desired linear position for thermal delivery. The rendered probe's rotary position can also be adjusted to the desired direction (angle) for thermal delivery. A scan plane can be selected under monitoring preferences of the workstation, and a thermal monitoring sequenced can be cued MRI system's sequence protocol list. The displayed scan plane parameters can be entered into the thermal monitoring sequences protocol's geometry parameters in the MRI.

An acquisition can then be started under a monitoring status bar of the workstation interface, and a thermal monitoring sequence on the MRI can be acquired. Under a noise masking heading of the workstation interface, 3 to 12, 4, 5, 6, 7, 9, 10, 11, 13 or 15-25 reference points, such as 8 reference points, can be selected at the periphery of the overlaid, orange noise mask in each of the three displayed image monitoring view-panes surrounding the intended thermal delivery area.

Once "Ready" is displayed under a laser status heading, a foot peddle of the workstation can be depressed to deliver thermal energy to the intended area of the brain. Thermal energy can be continuously delivered while monitoring created thermal dose contours overlaid onto the three thermal monitoring view-panes on the display screen of the workstation. Thermal delivery can be stopped when desired by releasing the foot peddle.

The MRI is allowed to continue to acquire the thermal monitoring sequence until the tissue returns to baseline body temperature. Stop acquisition can then be selected through the workstation to stop acquiring the thermal monitoring sequence on the MRI. These steps can then be repeated until a desired thermal dose is received by the entire, intended volume of tissue.

An exemplary procedure overview is shown in FIGS. 17-19, which includes algorithmic, computer-implemented processes and/or functions, together with operations performed by a user, technician, nurse and/or surgeon (or other physician or assistant). The steps shown herein generally include one or more sub steps consistent with the other portions or sections of this disclosure.

At S102, anesthesia is given to a patient. Anesthesia includes general and/or local anesthesia to sedate or put the patient under. The anesthesia may also merely numb or relieve pain, in some implementations. The patient's head is then fixated at S104. Before head fixation, a head coil and stabilization system can be utilized, as discussed in other portions of this disclosure. For example, a particular head coil and stabilization system is described in Section V.

The operation area of the patient's head is then draped to create a sterile field at S106. Such draping can include the placement of patches or sheets on and/or around the patient's head to minimize exposure and the chances for infection. After the sterile field has been established, a miniframe is attached to the patient's head at S108. A particular miniframe in accordance with this disclosure is described in Section II. The miniframe is aligned at S110. A probe entry location into the skull is identified, and a burr hole may be created prior to miniframe attachment or a twist-drill hole can be created

following stereotactic miniframe trajectory alignment. The twist-drill hole can have a size of 1-5 mm, 2 mm, 3 mm, 4 mm or 4.5 mm.

In this alignment, the trajectory and mainframe are adjusted so as to conform with a pre-planned trajectory for the insertion of a probe or other instrument into the patient's skull. Alignment at S110 can also include visual-based stereoscopic alignment with the assistance of three-dimensional renderings in an operating room. Such alignment can utilize instruments that include fiducial markers that specifically identify a three-dimensional position of the instruments relative to the patient's skull. Markers can include electronic (e.g., RFID—radio frequency identification) markers and/or visual markers.

At S112, the interface platform is attached to the head end of a head coil and stabilization system, as shown in FIG. 6, the patient is placed in an MRI, and a pre-planning procedure commences. The stabilization system can be attached to the patient on a patient table that moves with the patient between various rooms (including a surgical room, an operating room, and the MRI room). The patient can be immobilized using a head fixation ring. The patient's head should be secured with a head fixation device and remain fixed within the magnetic space for the entire imaging portion of the outlined workflow. In advance of each procedure, a data transfer interface should be enabled following patient registration on the MRI system. If the patient head position changes relative to the head fixation device at any point during the procedure the user should either register the patient in the MRI system as a new exam or use the MRI positioning lights to "re-landmark" the patient into magnet space center position. The entire head should be re-scanned to include the mainframe using a 3D volumetric scan. This scan should be co-registered with all other loaded planning sequences and be set as the master or thermal dose may be delivered in an unintended area causing patient injury. The head coil can be attached to the stabilization within the MRI room or in an operating room.

At S114, as part of a pre-planning procedure, image data is loaded from the MRI and a volume definition is generated and co-registered via the workstation at S116. Intended treatment region(s) of interest (ROI)(s) and initial trajectory(ies) is/are created and established as desired at S118. At the same time as the pre-planning procedure or after the trajectory definition is generated at S118, the MRI trajectory is confirmed at S120. This MRI trajectory can be confirmed via a wand that includes a material, such as a liquid, that is visible in the MRI image. The wand can be placed in the miniframe. Depending on a site specific workflow, the interface platform may be attached prior to or after the MRI trajectory confirmation at S120. The order of these steps is typically determined with the MRI or surgical support team during on-site training. Then, the IP power and motor plugs are connected, as shown in FIG. 10. Image data is then loaded and the trajectory is registered therewith at S122.

The miniframe includes fiducial markers that are detectable by the MRI such that image data includes the fiducial markers of the miniframe, and such that a position and orientation of the miniframe can be registered and detected by a workstation. At S124, the fiducial markers of the miniframe are detected by the MRI such that a position and orientation of the miniframe can be registered by a workstation. The established trajectory of the miniframe should be evaluated using MRI prior to inserting a probe into the brain. Volumetric imaging is recommended to include the entire head and full extent of the miniframe. This image data can also be used for treatment planning if pre-treatment image data is not available.

At S126, a maximum probe depth (PDP) is set. This maximum probe depth is set to reduce chances of inserting a probe or other instrument further into tissue of the patient than as previously planned, which can cause unintended damage to the tissue. An initial probe insertion depth is set at S128. Further aspects of the above pre-planning and setting and/or registration of probe depth and miniframe alignment are described in a particular implementation in Section VI.

A system self test commences at S130. This system self test can confirm operation and positioning of the various components discussed above. At S132, a foot pedal of the workstation is checked to confirm the foot pedal activates operation of, for example, a laser probe. At S134, a probe driver is attached to the miniframe, and alignment and positioning of the probe driver is checked with the workstation. Further, operation of the probe driver is verified. A particular implementation of a probe driver is described in Section III. A follower is attached to the miniframe, and a rotary test tool is attached to the follower to provide position feedback for a probe drive self-test step. Once the self-test step is determined as successful, the rotary test tool is removed by depressing a release button on its side and pulling it back off of the follower, as illustrated in FIG. 11b. Upon removal of the test tool, the rotary position will no longer be valid and will be displayed on the interface platform as "Unset" until a probe is placed into position.

A probe is attached and inserted into the probe driver and/or the patient's skull at S136. Particular implementations of the probe are described in Section IV. However, other types of probes or instruments can be utilized. Once an appropriate probe size is selected, a corresponding probe is removed from its sterile pouch and placed in the sterile field.

At S138, an MRI scan is conducted to ensure probe placement is correct and confirm delivery of the probe along the intended trajectory. Acquired image data with already loaded pre-planning image data (if any) can be loaded using a corresponding function (e.g., a graphical user interface) of the workstation. The rendered probe in the workstation can then be adjusted at S140 as needed to match the probe artifact on the acquired image to ensure that the alignment and arrangement of the probe as physically placed in the miniframe and inserted into the patient coincides with the rendered probe at the workstation. The rendered probe's trajectory can be adjusted to the desired linear position for thermal delivery. Further, the rendered probe's rotary position can also be adjusted to the desired direction (angle) for thermal delivery. Once the software rendered probe matches the probe artifact on the screen, "Yes" or "Confirm" can be selected through the workstation to confirm trajectory. A scan plane can be selected under monitoring preferences of the workstation, and a thermal monitoring sequence can be cued MRI system's sequence protocol list. The displayed scan plane parameters can also be entered into the thermal monitoring sequences protocol's geometry parameters in the MRI. Other aspects of this interface with the workstation is discussed in Section VI.

Treatment of a tissue can then commence, starting with setting up real-time transfer of MRI data, specifically imaging data, to the workstation at S142. At S144, real-time measurements can begin, and at S146, temperature calculation measurements can be set up and monitored. At this time, several images of a tissue to be treated are visible to a user at the workstation, and a probe is ready to be fired or activated to emit laser energy, for example, to the tissue to be treated. Under a noise masking heading of the workstation interface, eight reference points can be selected at the periphery of the overlaid, orange noise mask in each of the three displayed

image monitoring view-panes surrounding the intended thermal delivery area. Once "Ready" is displayed under a laser status heading, a foot pedal of the workstation can be depressed to deliver thermal energy to the intended area of the brain. Thermal energy can be continuously delivered while monitoring created thermal dose contours overlaid onto the three thermal monitoring view-panes on the display screen of the work station. Thermal delivery can be stopped when desired by releasing the foot pedal. At S148, the thermal dose of the laser is monitored, and effective treatment can be monitored. Further aspects are described in Section VI.

Once a thermal dose for a particular alignment and positioning of the probe is determined, the probe can be rotated at S150, and thermal dose monitoring at S148 can be repeated with various probe rotation alignments. Lasing (laser output) can then be terminated at S152, and the probe can be subjected to linear travel at S154 to various linear positions for creating an effective treatment region that is shaped to the to-be-treated tissue portion, by repeating steps S142-S154. Rotation and linear travel of the probe can be controlled by a probe driver, a particular implementation of which is described in Section III. The MRI is allowed to continue to acquire the thermal monitoring sequence until the tissue returns to baseline body temperature. "Stop acquisition" can then be selected through the workstation to stop acquiring the thermal monitoring sequence on the MRI. These steps can then be repeated until a desired thermal dose is received by the entire, intended volume of tissue.

Once treatment is completed the patient can be removed from the MRI bore at S156, and the probe and probe driver can be removed at S158. At this time, if another probe or probe driver is to be used, the procedure can be repeated by returning back to S110 to align the miniframe trajectory of the new probe and/or probe driver. Otherwise, the miniframe can be removed at S160, and the patient can be closed at S162.

In light of the descriptions provided herein:

An adjustable device, a miniframe, is provided that allows for a movable probe tilt point spaced apart from patient's head, while the miniframe is affixed to the patient's head. A probe attached to the miniframe can be advanced (laterally displace and/or rotated) under MRI guidance.

The head coil and stabilization system can fixate a patient and permit thermometry around substantially an entire crown line of the patient. In conjunction with the miniframe, steep and shallow probe insertion angles are available.

Multiple different probes can be utilized and swapped in the MRI room so as to provide different ablation patterns from different probes. For example, a symmetrical ablation probe can be used, followed by a side-fire (asymmetrical) ablation probe. A diffused tip probe can also be utilized.

A process of advancing probe, asymmetrically ablating, measuring, advancing probe and repeating is provided, such that the process does not require the interruption of a user-intervention in the MRI room to change probes or probe position.

Further, alterations to the procedures discussed herein can include the following:

The miniframe can be affixed in a preparation room, then placed in the MRI, and then the trajectory of the miniframe can be set in the preparation room. The hole can be drilled in the preparation room, and the patient can then be returned to the MRI for ablation procedure. This may proceed without an operation room (OR). The trajectory can also be optionally set based on images taken immediately prior to an ablation or treatment procedure. Further, a single burr hole and trajectory

can be utilized by the use of family of probes. The procedure(s) can optionally be conducted without general anesthesia.

The miniframe provides a movable pivot or tilt point above a target, i.e., above the patient's head. The probe driver is attached to the interface platform, as shown in FIG. 10, allowing control of movement of a probe or other implement attached to a probe driver follower to be rotated or longitudinally moved. Thus, a movable pivot or tilt point above a target is provided for a probe or other implement, which can be advanced or rotated under MRI guidance, through control by an operator or a workstation that is located in a separate room.

A trajectory can be set, after the miniframe and head stabilization system are attached to a patient, by utilizing an MRI to visualize a trajectory of the miniframe and set/register/lock the miniframe and/or the head stabilization system to an appropriate alignment. Then, a burr hole can be drilled in a prep room using the registered miniframe. The patient is then returned to the MRI for treatment procedures.

In some aspects, one or more burr holes, the head fixation components, and the miniframe are attached without the use of an operating room.

The trajectory can be adjusted immediately prior to a treatment procedure (e.g., an ablation procedure), based on recent MRI imaging.

Consistent with Section IV, a plurality of trajectories and/or probes can be inserted into a single burr hole. Also, pursuant with Section IV, a plurality of probes can be utilized with a single trajectory and a single burr hole.

II. Miniframe

The mini frame in an implementation coincides with the frameless trajectory guide described in US 2010/0042111, which is incorporated herein by reference in its entirety. The miniframe can also be modified to conform with the examples shown and discussed herein.

FIG. 20 illustrates a miniframe 200, which can also be referred to as a frameless trajectory guide or simply as a trajectory guide. The miniframe 200 includes a tilt portion 202 and a rotation portion 204. The miniframe 200 also includes a plurality of legs 206.

FIGS. 21 and 22 illustrate two different rotational positions of the rotation portion 204. As shown in FIGS. 21 and 22, a rotation of the rotation portion 204 does not necessarily change the actual trajectory of the a through hole 208 of the tilt portion 202, through which an instrument, such as a probe, is insertable therein. The through hole 208 includes two alignment guides 264. These alignment guides 264 allow for proper pre-determined alignment between a probe and/or a probe follower and the miniframe 200.

Rotation of the rotation portion 204 can be locked via a cam 210. FIG. 23 illustrates a locked position of the cam 210, whereas FIG. 24 illustrates an unlocked position of the cam 210. In the unlocked position, the rotation portion 204 is free to rotate. On the other hand, in the locked position, the rotation portion 204 is inhibited or stopped from being rotated.

FIG. 25 illustrates an exemplary cam in accordance with the shown implementation. The cam 210 includes a plurality of teeth 212. These teeth 212 are structured so as to engage corresponding teeth of the rotation portion 204, discussed below.

The rotation portion 204 includes a frame 214. The frame 214 includes a plurality of mounts 216 that are arranged so as to be coupled to the legs 206. Further, the frame 214 includes a cam mount 218 that is arranged to receive the cam 210.

FIG. 27 illustrates a retaining ring 220, which includes a tab portion 222 and a plurality of alignment markings 224. The tab portion 222 is arranged so as to coincide with the cam

mount **218** and the cam **210**, as shown in FIGS. **23** and **24**, for example. Further, the tab portion **222** provides a rotational stop to limit rotation of movement of the cam **210**, as shown in FIG. **24**, by example.

FIGS. **28** and **29** illustrate top and bottom perspective views of a central housing **226** of the rotation portion **204**. The central housing **226** includes a plurality of teeth **228** that are arranged to engage the corresponding teeth **212** of the cam **210**.

The engagement and non-engagement of the cam **210** to the central housing **226** is illustrated in FIGS. **30-33**. FIGS. **30-31** illustrate an unlocked engagement, where the rotation portion **204** is free to rotate. FIGS. **32-33** illustrate a locked engagement in which the teeth **212** of the cam **210** create a locking engagement with the teeth **228** of the housing **226**, as shown by the underside view of FIG. **33**.

With the above locking mechanism provided by the cam **210** and the housing **226**, relative rotation between the rotation portion **204** and the frame **214** is inhibited. The frame **214** is mounted via the legs **206**, where the legs **206** provide an initial trajectory, which is defined by a placement of the legs **206**, a length of the legs **206**, and initial positions of the rotation portion **204** and the tilt portion **202**. In one implementation, a tilt angle of the tilt portion **202**, a rotation angle of the rotation portion **204**, and lengths and placements of the legs **206** are set to a pre-planned trajectory, and the miniframe is **200** mounted to a patient's skull. For example, the rotation angle of the rotation portion **204** and the lengths and placements of the legs **206** can be set, and then the miniframe is attached to the patient. Thereafter, the tilt angle of the tilt portion **202** is set.

FIGS. **34** and **35** illustrate two different exemplary tilt angles of the tilt portion **202**. Together, the tilt portion **202** and the rotation portion **204** can form a spherical shape, in which rotation and tilt are independently controlled and independently locked. The above description provided for the locking mechanism for rotation. The following describes a locking mechanism for tilting.

FIGS. **36** and **37** illustrate, respectively, locked and unlocked positions of locking arms **230** of the central housing **226** of the rotation portion **204**. FIG. **36** illustrates a squeezed position in which locking arms **230** are squeezed together at tabs **232**. As shown in FIG. **37**, an unlocked position can be achieved by depressing the non-tabbed ends **234** of the locking arms **230**. FIGS. **38-39** illustrate opposing prospective views of one of the locking arms **230**. One of the locking arms **230** can be a mirror image of the other of the locking arms **230**.

The locking arms **230** are provided on opposing sides of the tilt portion **202**, as shown in FIG. **40**, so as to pivot or rotate about a rotational engagement between the locking arms **230** and the tilt portion **202**. Adverting back to FIGS. **36** and **37**, it can be seen here that the central housing **226** of the rotation portion **204** covers the rotational engagement between the locking arms **230** and the tilt portion **202** when the central housing and the rotation portion **204** are assembled together.

FIGS. **40-41** illustrate an unlocked position between a locking arm **230** and the tilt portion **202**. Similar to the cam **210**, the locking arm **230** includes a plurality of teeth **236**. The tilt portion also includes a plurality of teeth **238** that are arranged to engage and create a locking engagement with the teeth **236** of the locking arm **230**. FIGS. **42-43** illustrate a locked engagement.

FIGS. **44** and **45** illustrate top and bottom perspective views of the tilt portion **202**. The tilt portion includes a plurality of markings **238** for tilt alignment measurements, as

well as a rotational axis **240** that is arranged to rest within a corresponding recess **242** provided in the central housing **226**, as shown in FIG. **29**.

FIG. **45** illustrates a fiducial marker **244** that is included in the tilt portion **202**. This fiducial marker **244** can be arranged coaxially with the through hole **208**. The fiducial marker **244** can be utilized via MRI imaging for trajectory verification. The fiducial marker **244** can include a fluid that is MRI visible. A diameter of the fiducial marker can be about 5.25 mm.

Adverting back to FIG. **20**, the rotation portion **204** can include first and second alignment lines **246**. The alignment markings **224** can be spaced every 10° and can be arranged so as to coincide with the first and second alignment lines **246** with respect to determining a rotational position of the rotation portion **204** and the tilt portion **202**. The first and second alignment lines **246** can also coincide with tilt markings **248**. These tilt markings **248** can be staggered and spaced several degrees apart, with respect to left and right sides, to limit the number of markings on the tilt portion **202**. The tilt markings **248** can be spaced apart by 1°, 2°, 5°, 10°, 20°, 30° or 1-30°. Similarly, the first and second alignment lines **246** can be staggered by several degrees in the rotation and tilt directions to limit a number of alignment lines on the various components. The lines **246** can be spaced apart by 1°, 2°, 5°, 10°, 20°, 30° or 1-30°.

The legs **206** can resemble the legs described in US 2010/0042111. However, modifications can be made. FIGS. **46-47** illustrate a foot **250** of a leg **206**. The foot **250** and the leg **206** can be coupled together by a ball-socket joint **252** that allows for both rotational and tilt motion therebetween. The joint **252** can include a spherical structure that extends from either one of the legs **206** or the foot **250**. In the implementation shown, the spherical shape extends from the leg **206** and is coupled to the foot **250** by a foot cap **254**. The foot cap **254** can be removed from the foot **250** using a twist bayonet-type locking mechanism. An unlocked position is shown in FIG. **46**, whereas a locked position is shown in FIG. **47**. In the locked position, relative movement between the leg **206** (the joint **252**) and the foot **250** is impeded by a frictional engagement, whereas the frictional engagement is lessened and/or removed outright in the unlocked position of FIG. **46**. The cutouts **268** have an angled edge which assists in keeping the foot cap **254** in the locked position via the protrusion **256**. In the locked position, the protrusion **256** is held at a first position within the cutout **268**. The foot cap **254** is moved to an unlocked position by twisting the foot cap **254** to cause the protrusion **256** to progress an inclined or angled edge **270** of the cutout **268** until the protrusion traversed the angled edge **270**, and the foot cap **254** can decoupled from the protrusion **256**.

FIG. **48** illustrates the foot **250** as being completely disconnected from the leg **206** and the foot cap **254**. As shown herein, the foot **250** includes protrusions **256** that are inserted into respective cutouts **268** of the foot cap **254**, as well as a protrusion **258** that is arranged to maintain at least a loose coupling between the foot cap **254** and the foot **250**, when the foot cap **254** is in an unlocked position. The foot **250** can also include a plurality of spikes **260** about 0.1-1.5 mm, such as 0.4, 0.5, 0.6, 0.8 or 1.0 mm in length, which may be made from a titanium material. The titanium material is strong and sharp and will not bend when being pressed into the skull. Further, a straight profile of the spikes **260** reduces the resistance when being pressed into the scalp. The spikes **260** can be molded into the foot **250**, which is also made of plastic or titanium. Prior to installation, as shown in FIG. **49**, the spikes **260** can be covered by a spike plate **262**. FIG. **50** illustrates the

spike plate **262** by itself, and FIG. **51** illustrates a titanium spike **260** by itself. In FIG. **51**, the titanium spike **260** is shown as including a nail portion **264** and a grooved portion **266**. Several grooves are provided to create a rigid and reliable connection between the foot **250**, which can be a molded plastic, and the titanium spike **260**.

FIGS. **52-54** illustrate various views of the foot cap **254** having the cutouts **268**. FIGS. **52** and **54** illustrate respective bottom and top perspective views of the foot cap **254**, and FIG. **53** illustrates a side view of a foot cap **254**. As shown in FIG. **53**, the cutouts **268** include the angled edge **270** to promote a locked position with the protrusions **256**.

Although not shown, the spike plate **262** can include holes and/or grooves so that a sterilization gas can contact the titanium spikes, which are intended to be inserted into a patient's skull. Such a sterilization gas can be, for example, ethylene oxide. Further, leg numbers can be added to the frame **214** and/or the retaining ring **220** such that identification of a particular leg of the miniframe can be easily identified from a look-down position. Further, the spikes **260** can be varied in length based on a particular placement, and the foot **250** can be increased in size to create a larger footprint to extend around areas where screws and/or spikes cannot be attached to a patient's skull.

Although a preferential order of alignment of the various components can include positioning and securing the legs **206**, then rotating the rotation portion **204**, and then adjusting the tilt portion **202**, orientation of the miniframe **200** can be made following a different order of steps, without diverting from the steps of this disclosure. For instance, fiducial markers can be attached to the patient's skull to map a three-dimensional surface profile of the patient's skull, and the tilt and rotation and leg **206** lengths of the miniframe **200** can be calculated prior to mounting the miniframe **200** to the patient's skull. Once the calculations are verified, verification of the calculations being performed by modeling a rendered miniframe **200** or placing an actual miniframe **200** having the calculated settings applied thereto to the patient's skull either in the physical space or in the rendered space. Once verified, then the miniframe can be attached via spikes or screws to the patient's skull, and the trajectory can then be verified through MRI scanning or optical imaging.

In light of the above, it should be appreciated that the independently rotating and tilting portions of the miniframe can simplify adjustments, wherein a tilt-point (i.e., the tilt portion **202**) is provided so as to be displaced from a patient's skull. The tilting and rotational portions can also be independently locked with non-friction (i.e., non-pressure based) locks. That is, teeth locks can be independently provided for each of the tilting and rotational portions. Pressure/friction-based locks/holders can be utilized to secure a probe and/or a probe driver or other instrument engaged with the miniframe via the tilting portion. The miniframe can be a single-use, disposable component, in that a miniframe is used per patient. A single miniframe is usable with multiple probes, trajectories and procedures in succession for the patient.

The miniframe provides full rotational freedom of the rotating part and the tilt portion, and a wide range of tilt angles for the tilt portion. The locking mechanisms can be easily released and reset. Thus, a trajectory can be modified and re-locked in real-time based on real-time image data or to set a next trajectory in a treatment procedure.

In planning, setting, registering or modifying a trajectory, an MRI-visible portion of the miniframe (such as the fiducial marker **244**) can be used, via MRI imaging, to verify a position of the mini frame, especially with respect to a target tissue or intended trajectory. Moreover, a further MRI-visible

portion, such as a fluid filled tube, can be placed in the through hole **208** or in a device that is inserted into the through hole **208** to provide an MRI-visible indication of trajectory of the miniframe.

The miniframe provides a tilt/pivot point that is in a different radial position than an entry point, with respect to a spherical coordinate system.

III. Probe Driver

An exemplary probe driver that can be utilized in accordance with the various aspects presented in this disclosure is described in U.S. Ser. No. 12/540,558, filed Aug. 13, 2009, published as US 2010/0042112, the entirety of which is incorporated herein by reference.

An exemplary probe driver is shown in FIG. **5**. FIG. **5** illustrates the probe driver as including a commander, connected to a follower by umbilicals, and a position feedback plug connected to a potentiometer assembly of the follower. The position feedback plug is plugged into an interface platform and the umbilicals include sheathed wires that independently control rotational and longitudinal motion of a probe or other longitudinal member held by the follower. Independent control of the rotational and longitudinal motion is provided by rotating a respective one of the knobs or dials provided at either side of the commander. An exemplary structure for the corresponding mechanisms that provide the rotational and longitudinal motion is described and shown in U.S. 2010/0042112. The entirety of which is incorporated herein by reference.

FIG. **55** illustrates a commander **300** of an exemplary probe driver. The commander **300** includes opposing knobs or dials **302** and **304** (herein knobs **302** and **304**). These knobs **302** and **304** independently control longitudinal and rotational motion, e.g., in a manner that coincides with that described in the exemplary structure of US 2010/0042112. The commander **300** is arranged to be mounted to an interface platform body, as shown in FIG. **55**, via corresponding holes and mounting posts.

The knobs **302** and **304** each include gear teeth that are structured to be engaged with corresponding gear teeth **306** and **308** of the interface platform. The interface platform includes motors to respectively rotate the gear teeth **306** and **308** in response to corresponding instructions (data) received from a workstation in an MRI control room (see FIG. **1**). When the commander **300** is coupled to the interface platform, rotation of the gear teeth **306** and/or **308** is translated to the gear teeth of the knobs **302** and/or **304**, which results in independent control of the rotational and longitudinal motion.

FIG. **56** schematically illustrates either of the knobs **302** and **304** engaged with the interface platform via an engagement between the teeth **310** of the knobs **302** and **304** and the teeth **306** and **308** of the interface platform. Either or both of the knobs **302** and **304** include a contoured surface **312** for manual manipulation thereof, as well as a bolt or fastener **314** that secures the knobs **302** and **304** to internal mechanisms of the commander **300**.

Other engagements are also possible, including toothless friction rollers. With any type of engagement, a rotational motion originating from a workstation, that causes the gear teeth **306** and/or **308** (or other interface platform rotational driving mechanism) to rotate, causes the knobs **302** and/or **304** to rotate. Consequently, rotational and/or longitudinal movements via the follower are enacted. These movements are then tracked via a potentiometer assembly in the follower, and a feedback signal is provided to the interface platform. Consequently, a workstation receives electronic positional feedback and is able to verify that an instructed command

resulted in an intended rotational and/or longitudinal alignment, and can responsively output further commands to the commander to achieve an intended alignment, should the initial command not result in a particular or intended position. The workstation monitors such unintended alignments to determine whether an amount of slippage in the various mechanisms is above a certain tolerance, and displays a warning error so that the mechanisms can be visually inspected to ensure proper setup and functioning.

In conjunction with electronic control provided via the workstation, a clinician at the workstation, which is coupled to the probe driver via the electronics rack and the interface platform, is provided with an automated drive means that is spaced apart from the MRI (that is, outside of the bore of the MRI), but is coupled to a flexible MRI-compatible umbilical, which is in turn coupled to a motorless drive system positioned within the bore of the MRI and/or a head coil positioned around the head of a patient. Actuation of the drive means can therefore be accomplished by a clinician who is not in the MRI room, but is rather in a control room, such as an MRI Control Room, and control of the motorless drive system can be provided while the MRI is operating and images are being collected. Further, continuous, uninterrupted control of neural laser ablation (or other treatment depending on the probe structure) is possible when the probe in use requires repositioning. That is, in a multi-step treatment, e.g., a multi-step ablation, operation of the MRI can be continuous while a probe position is changed in either or both of rotational and longitudinal directions.

In various implementations the probe driver provides full remote control to an operator that is located either: (1) in the proximity of the MRI and an interface platform that the probe driver is connected to, or (2) in a remote room, such as a control room, at a workstation, where the workstation sends positioning signals to the interface platform to actuate corresponding movements by the commander. Full remote control of the probe drive is thus provided, which reduces procedure time.

Further, the probe driver in this illustrated implementation can provide, at a minimum, a translation of 20-80 mm, 30-70 mm, 40-60 mm or 40 mm, with a maximum translation of 60 mm, 80 mm, 100 mm, 120 mm or 60-150 mm or more. The probe driver in this illustrated implementation can also provide, at a minimum, a rotation of 300°-340°, with a maximum rotation of 350°, 359°, 360°, 540°, 720° or more or of any angles therebetween.

IV. Probe

A plurality of different probes can be utilized in accordance with the various aspects presented in this disclosure.

Exemplary probes are described in: U.S. Pat. No. 8,256,430, filed Dec. 17, 2007; U.S. Pat. No. 7,691,100, filed Aug. 25, 2006; U.S. Pat. No. 7,344,529, filed Nov. 5, 2003; U.S. Pat. No. 7,167,741, filed Dec. 14, 2001; PCT/CA01/00905, filed Jun. 15, 2001, published as WO 2001/095821; U.S. 61/728,068, filed Nov. 19, 2012; and U.S. 61/664,791, filed Jun. 27, 2012. These documents are incorporated herein in their entireties.

A. Side-fire Probe

FIG. 57 illustrates an exemplary side-fire probe tip 400 (herein sometimes referred to as merely a probe 400). Probe 400 includes a cooling tube 402 and thermocouple 404. As shown in FIG. 3, these components are coupled to corresponding probe connectors that are secured to the interface platform, as further shown in FIGS. 10 and 14. The probe 400 also includes an optical fiber 406 as an active element. The cooling tube 402, the thermocouple 404 and the optical fiber 406 are enclosed in a capsule 408. In one implementation, the

capsule 408 is a sapphire capsule. However, other materials can be used, including quartz. Further, when a non-laser probe or a non-light-based probe is utilized, a material suitable for ultrasound or radio frequency transmission can be used, and such a material can be the same as that used for the cannula. Otherwise, other crystal structures or glass-type structures can be utilized that effectively transmits light, without allowing for an effective amount of reflected light, when a laser probe or other light-based probe is utilized. Further, such materials can include coatings and films, such as optical films.

The optical fiber 406 includes a sheathed portion and an unsheathed portion 410. The unsheathed portion 410 includes a faceted end surface 412, which causes energy, such as laser energy, to be directed in the direction of arrow 414 to initiate therapy in a tissue. Therapy can include, for example, heating or light exposure. When heating a tissue, to control an amount of therapy or heat applied to the tissue, cooling is provided via the cooling tube 402, which outputs a cooling gas or fluid to the expansion chamber 416. The thermocouple 404 detects a temperature in the expansion chamber 416. A workstation can control an amount of cooling gas (either or both of a flow and pressure of the gas) or cooling fluid inputted into the expansion chamber 416 via the cooling tube 402 to control a temperature of the tissue via conduction through the capsule 408.

In one implementation the optical fiber 406 is rotatable with a rotation of the probe 400, for example, by rotating a follower of a probe driver. In another implementation, the optical fiber 406 is independently rotated by the follower, such that rotation of the optical fiber 406 does not necessitate rotation of the capsule 408. As a result of the side-firing capability of the laser energy, a plurality of rotationally different portions of the tissue can be treated with the laser energy by rotating the optical fiber 406 with or without rotating the capsule 408. Additionally, the capsule 408 can be longitudinally displaced by a follower of a probe driver to change a longitudinal position of the directionality of the laser energy within a tissue to be treated. This longitudinal movement of the capsule 408 results in movement of the cooling tube 402, the thermocouple 404, and the optical fiber 406 as one piece.

In another implementation, the optical fiber 406 can longitudinally move with respect to the capsule 408. Consequently, movement of the laser energy from the optical fiber 406 in the longitudinal direction can be achieved without moving the capsule 408 or other parts thereof.

The optical fiber 406 can be referred to as a core of an optical laser fiber. A tip of the core can be polished at an angle of 38 degrees to provide an exemplary side-fire probe.

B. Diffuse-tip Probe

FIG. 58 illustrates a diffuse-tip probe 420 (herein sometimes referred to as merely a probe 420). The probe 420 includes some components that are similar to that of probe 400. The probe 420 includes an optical fiber 422 that has a sheathed portion and an unsheathed portion 424. The sheath can be formed from a polymeric material such as nylon, ethylene-tetrafluoroethylene, polyamines, polyimides, and other plastics known for optical sheaths or jackets. The unsheathed portion 424 includes a faceted surface 426. The faceted surface 426 results in a diffused output of energy in a side-firing direction, such as in the direction of arrows 428.

The faceted surface 426 is an etched fuser tip, from which laser energy, for example, is delivered diffusely in an even or uneven distribution pattern into a tissue. A longitudinal length of the faceted surface 426, in a longitudinal direction, can be approximately 1, 1.4, 2, 3, 4-30 or 45-60 mm. A plurality of similarly structured diffused-tip probes can be provided with

varying active lengths, where a particular active length can be selected based on a particular tumor size to be treated. An exemplary length is 6 mm or 4-7 mm.

With respect to the described examples, in general, the unsheathed portion of the optical fibers described herein includes a cladding, whereas the faceted surface(s) of the unsheathed portion do not include the cladding. Additionally, the faceted surface(s) can be etched by, for example, an acid treatment. In another implementation, one or more faceted surfaces are replaced by etched surfaces, in which the general structure of the optical fiber is maintained, but a clad is not present or removed, and the material of the optical fiber is etched to create one or more emission points. These emission points can be disposed along a longitudinal axis and/or circumferentially to form a symmetric or asymmetric energy emission pattern.

The capsule **408** can be fixed to a rigid cannula **418**, and the capsule **408** can be made of quartz, sapphire or other such suitable materials. The rigid cannula **418** is formed of a suitable rigid MRI compatible material such as plastic so that it is stiff in resistance to bending and has sufficient strength to allow a surgeon to insert the cannula into a required location in the body of a patient. In another implementation, the rigid cannula **418** is only rigid in a torsional, rotational direction, and is flexible at one or more points so that it is bendable.

The cooling tube **402**, the thermocouple **404** and the optical fiber can be attached by an adhesive to the cannula **418**. The cooling tube is swaged at its end and projects into the capsule **408** to form a cross section of reduced inner diameter on the order of 0.002, 0.003, 0.004, 0.003 to 0.005 or 0.006 inches or values therebetween. The capsule **408** can include a step portion **430** that can be pressed fit and/or adhesively secured to the cannula **418**. An outer diameter of the cannula **418** and the capsule **408** is the same, and an inner diameter of the capsule **408** and the cannula **418** is the same. However, the diameters can be varied. Additionally, a fiber optic thermometer, not shown, can be utilized instead of the thermocouple **404**. The cooling tube **402** can supply pressurized carbon dioxide, for example, and the supplied fluid/gas can utilize Joule-Thomson cooling via Joule-Thomson expansion. However, cooling fluids which do not expand but rather circulate from the cooling tube **402** through a discharge duct can also be used.

A fluid supply for the cooling tube **402** originates from the electronics rack shown in FIG. 1. The electronics rack is coupled to the interface platform, which is in turn connected to the cooling tube **402** via the probe connectors shown in FIGS. 3 and 14. Similarly, the optical fiber and the thermocouple are connected to the electronics rack. Via the electronics rack, the workstation controls the flow rate of carbon dioxide, for example, in a cooling tube **402** to generate a predetermined pressure within the cooling tube **402**, which can be varied so as to vary a flow rate of the fluid through a neck portion of the cooling tube **402**. As a result, a Joule-Thomson effect is achieved, where gas exiting the reduced diameter neck portion expands into the expansion chamber **416** to cool the probe in contact with the tissue and cool the tip of the optical fiber that emits laser energy (such as the diffused tip portion provided by the faceted surface **426**). The cooling fluid can be supplied at a normal or room temperature without cooling. The fluid is normally a gas at this pressure and temperature. Fluids that are liquid can also be provided such that they form a gas at the pressures from the expansion chamber **416**, and therefore go through an adiabatic gas expansion process through the restricted orifice into the expansion chamber to provide the cooling effect. The restricted orifice or neck portion of the cooling tube **402** is

therefore a venturi outlet and has a cross-sectional area that is smaller than a main-body of the cooling tube **402**.

The interior of the probe serves as a return duct which discharges the cooling fluid/gas/liquid. An exhaust duct area of approximately 190 to 540 or 200 to 300 or 200 times larger than an orifice area of the cooling tube **402** can be achieved when considering a delivery orifice diameter of an exemplary 0.004 inches, or an exemplary 0.002, 0.003, 0.004, 0.003 to 0.005 or 0.006 inches or values therebetween. Cooling of at least -20° C. to $+20^{\circ}$ C. is achieved with at least a 200:1 (outlet:inlet) gas expansion ratio. This allows the gas, as it passes into the expansion chamber, to expand as a gas, thus cooling the capsule **408** and an interior thereof to a temperature in the range of at least -20° C. to $+20^{\circ}$ C. This range of temperatures has been found to be suitable in providing the required level of cooling to the surface of the capsule **408**, so as to extract heat from the surrounding tissue at the required rate of cooling. Variations in the temperature range are achieved by varying the pressure of the cooling gas/fluid so that in one example the pressure of the gas is between 700 and 850 psi and has a flow rate of 1, 2, 3, 4, 5 or 6-15 liters per minute. Other achievable temperature ranges include -40° C. to $+40^{\circ}$ C., -35° C. to $+35^{\circ}$ C., -30° C. to $+30^{\circ}$ C., -25° C. to $+25^{\circ}$ C., -15° C. to $+15^{\circ}$ C., -10° C. to -10° C., and ranges therebetween. Other exemplary pressures of the gas include 600-650, 650-700, 700-750, 750-800, 800-850 and 700-900 psi.

To achieve a desired rate of cooling a probe is cooled to between 0° C. to 5° C., such as 1° C. to 3° C. or 2° C., by Joule-Thomson cooling. This temperature range is preferably maintained within an entirety of the probe before, throughout, and after a treatment or energy emission of the probe.

A discharge of the cooling gas through the cannula **418** is at a pressure of approximately 25-50, 75 or 50 psi in the example described herein. Thus, the gas may be discharged through the atmosphere if the gas is inert, discharged to an extraction system, or collected for cooling and returned if economically desirable. Cooling of the probe is necessary for optimum tissue penetration of the laser or heating energy. Cooling reduces tissue charring and sets localized cooling of the treated region. Probe cooling also protects the faceted surface or an otherwise active area of the optical fiber. The faceted surface **426**, in the longitudinal direction, is shorter than an internal length of the capsule **408** so that the faceted surface **426**, which defines the active length, can be approximately centered within the expansion chamber **416**, and so that no or little to no energy is delivered to the sheath of the optical fiber. The faceted surface **426** is arranged such that it is surrounded by the cooling gas from the cooling tube **420** within the expansion chamber **416**. As a result, in practice, no condensate forms on the faceted surface **426** that would otherwise interfere with reflective characteristics.

In operation, the temperature of the expansion chamber **416** is monitored by the thermocouple **404** so as to maintain the temperature at a predetermined level in relation to an amount of heat energy supplied through the optical fiber. Pressure of the cooling gas is varied to maintain the temperature at the predetermined set level during a hypothermic process.

FIGS. 59-66 illustrate alternative faceted surfaces or active areas for diffused-tip type probes. In these figures, the structures can be considered as being drawn to scale. The structures can also be considered as accentuated in size so that their shape is readily understood. Accordingly, in some aspects, the drawings can be considered as schematic in nature and as not being drawn to scale. Further, an effective/active area for laser-energy emission is shown by hash marks. In one imple-

mentation, the area of the optical fiber that is not sheathed and is not shown by hash marks includes cladding.

FIGS. 59 and 60 illustrate an implementation that includes a faceted surface/active area 432 that ends in a clad portion that comes to a tip 434. FIG. 59 is a side profile view of the faceted surface 432, where FIG. 60 is a view in which the faceted surface 432 is facing outwards. The faceted surface 432 includes one or more edges, in section, that can form a single inclined surface, a plurality of inclined surfaces, or a plurality of stepped portions.

FIGS. 61 and 62 illustrate a plurality of side-firing points 436. FIG. 61 is a side profile view of the faceted surfaces providing these points 436, whereas FIG. 62 is a view in which the points 436 face outwards. The implementation shown in FIGS. 61 and 62 provide a plurality of longitudinally displaced side-firing points. The points 436 are formed by recess, which can have an angular (as shown) or a curved (not shown) section. The points 436 can also be formed by merely etching surfaces of the optical fiber.

FIGS. 63 and 64 illustrate a structure that is similar to that shown in FIGS. 61 and 62. However, in FIGS. 63 and 64, the faceted surfaces are structured differently. In particular, the faceted surfaces of FIGS. 61 and 62 are a plurality of recesses 438 that form a saw tooth pattern. The difference in patterns between these two implementations varies a pattern of energy output. One may be preferable over the other for a particular tissue treatment shape or for a particular tissue shape/position.

FIGS. 65 and 66 illustrate a further modification to the saw tooth pattern shown in FIGS. 63 and 64. In particular, FIGS. 65 and 66 illustrate a graduated saw tooth pattern where individual recesses 440 vary in size. The varying in size shown in these figures is shown as increasing as the optical fiber approaches its end. However, other variations are possible. In particular, a size of individual recesses included in an optical fiber can be varied to achieve a prescribed laser energy output profile. Further, if merely etching is utilized, a size of the etching can be varied among a plurality of longitudinally spaced active areas on the optical fiber, where a clad separates each of the active areas.

The particular implementations shown in FIG. 61-66 include three separate longitudinally displaced side-firing points. However, two or more side-firing points, such as any one of 2, 3, 4, 5, 6, 7, 8, 9 or 10 or more points can be provided.

Consequently, an energy emission member is provided which includes a plurality of longitudinally displaced points of energy emission, which can be tuned, by either surface treatment or recesses, to achieve a prescribed side-firing profile of energy emission.

Compared to a non-diffused-tip probe (a non-DTP), a DTP can output a side-firing profile of energy that has a much larger longitudinal length within the tissue. By increasing an amount of energy of the DTP, an amount of heat generated within a larger portion the tissue can be increased, relative to a non-DTP. Therefore, a temperature of the tissue can be increased at a greater rate with the DTP than with the non-DTP. Further, with effective cooling by the probe, an amount of heat generated by a portion of the DTP can be canceled out by the cooling. Consequently, a more steady-state temperature of portions of tissue surrounding a target area can be provided, and the portions of the tissue surrounding the target area can be prevented from cooling by an effective amount.

The structure of the DTP provides a combination of higher energy output and lower energy density, when compared to a non-DTP probe (such as a side-tire probe). A larger treatment area can be treated within a shorter time window, when compared to the non-DTP probe.

C. Symmetric Probe

FIGS. 67 and 68 illustrate a symmetric probe with a symmetrical optical fiber having a curved or rounded faceted end 442. FIGS. 67 and 68 illustrate different sides of the optical fiber. FIGS. 69 and 70 illustrate another symmetrical optical fiber, showing different sides of the optical fiber, where the optical fiber has a flat faceted end 444. The ends of optical fibers shown in FIGS. 67-70 can include etching at ends 442 and 444.

The symmetric probes illustrated in FIGS. 67-70 provide symmetric ablation patterns, in which laser output is symmetric with respect to the longitudinal axis of the optical fiber.

The rounded end 442 shown in FIGS. 67 and 68 can provide a spherical or partial spherical laser light output, whereas the optical fibers shown in FIGS. 69 and 70, with the flat faceted end 444, can provide a point output.

Further, the other optical fibers described above can be modified to provide a symmetric output by providing a symmetric active area around a circumference of the optical fibers.

D. Guide Sheath

FIG. 71A illustrates an exemplary guide sheath 446. The guide sheath can include a capsule 448 which is made out of a material that is the same as the capsule 408 or the cannula 418. The guide sheath 446 can include a plurality of probes 450, where each of the probes 450 includes a different probe tip 452. In the illustration of FIG. 71A, only one probe 450 is shown for simplicity. By rotation of the guide sheath 446 and/or the individual probes 450, treatment of a same or different tissue portion of a patient can be affected by one or more of the probes 450. Consequently, only one bore hole and guide sheath insertion is used/needed to allow for treatment of a tissue by the plurality of probes that are simultaneously inserted into the guide sheath 446. The guide sheath 446 shown in FIG. 71A is straight and rigid. However, the guide sheath can also be curved to accommodate a given trajectory. Additionally, the guide sheath 446 can include one or more off-axis delivery hole(s) 454. The off-axis delivery hole 454 allows for a probe to be extended therethrough via contact surface 456. Such a structure allows for flexibility in targeting particular tissues in the patient.

The contact surface 456 has a predefined angle, and the off-axis delivery hole 454 is predisposed. The angles shown in FIGS. 71A and 71B can be considered as drawn to scale in one implementation. However, the alignment of the contact surface 456 and the hole 454 can be varied by adjusting their respective axial angles. By adjusting these angles, a plurality of possible positions of a probe 450, for insertion into a tissue through the hole 454, are provided. Further, multiple holes and multiple contact surfaces can be provided, which are displaced from each other in a direction of the longitudinal axis of the guide sheath 446.

FIG. 71B illustrates two probes 450a and 450b that are simultaneously inserted into the guide sheath 446 and can affect treatment of a tissue independently or at the same time. The two probes can provide either or both asymmetrical (side-fire type probe) and symmetrical (point or spherical ablation type probe) treatment patterns. As shown in FIG. 71B, the contact surface 456 can direct a probe tip 452a of the probe 450a through the hole 454. The probe tips 452a and 452b can be commensurate with any of the probes, probe tips and optical fibers described herein.

The probes 450a and 450b can be independently or collectively controlled with respect to axial/longitudinal movement and/or rotational movement. Further, one of the probes 450a and 450b can be dedicated to cooling, whereas the other of the probes 450a and 450b can be dedicated to laser treatment. A

cooling probe includes a cooling tube, temperature sensor and an expansion chamber in accordance with the descriptions provided herein.

The cannula of the probe **450a** shown in FIG. **71B** is flexible with respect to bending, such that the surface **456** causes the probe tip **452a** to extend through the hole **454**. A material for the cannula for the probe **450a** can be selected such that the probe **450a** has high torsional rigidity, and such that rotational movements of the probe **450a** are effectively translated to the probe tip **452a**. Additionally, a mesh joint or other type of joint can be utilized in at least a portion of the cannula for the probe **450a** that allows for bending, but maintains torsional rigidity.

A side-fire probe can provide an asymmetrical treatment pattern, whereas a point or spherical ablation probe can provide a symmetrical treatment pattern. Multiple probes of either or both functions are inserted into a common sheath. With respect to the multiple probes illustrated in FIG. **71B**, various exemplary sequences are available for an order of treatment. In particular, one probe can provide a symmetrical treatment pattern to affect a tissue, which can be followed by an asymmetrical treatment pattern. Further, a spherical ablation can then be followed by another probe, such as probe **450a**, by treatment via an off-axis hole in a guide sheath. This other probe can be a symmetrical, asymmetrical or other type of probe.

With reference to FIG. **71B**, this other probe can be the probe **452a**, which can then be rotated. The probe tip **452a** can also be retracted, the guide sheath **446** can be rotated, and then the probe tip **452a** can be extended to continue another step of treatment. The probe tip **452a** can be a symmetric or asymmetric probe tip.

The order of the above sequences can be altered.

The hole **454** can be provided at a tip/end of the guide sheath **446**, and probes within the guide sheath **446** can be independently rotated with respect to the guide sheath **446**. The probes can be rotated after being inserted through the hole **454** and/or before being inserted through the hole **454**. The hole **454** can also be provided at various locations to alter a deflection angle, with respect to a longitudinal axis, of a probe inserted therethrough.

The guide sheath can be straight or designed to provide a fixed angle off-axis delivery. The guide sheath can also be curved. Trajectories can be planned that include multiple guide sheaths, including multiple burr holes, multiple trajectories and multiple guide sheath introductions.

E. Probe Modifications and Procedure Considerations

A family of probes can be defined as catheters which differ from one another with respect to one or more of the following variables:

i. A number of probes simultaneously positioned in a guide sheath, including one or more probes. With multiple probes, the probes can be provided with group or individual axial movement and/or rotation, one or more of the probes can be dedicated to cooling only, and probes can be individually extended and retracted from the guide sheath.

ii. Diffuse or point emission.

iii. Symmetrical or asymmetrical emission.

iv. Axial or off-axis probe delivery.

v. Steerable head, where the probe includes a structure that can change a course or trajectory of the probe with respect to a trajectory defined by a guide sheath or other axial guiding structure.

Examples described include those relating primarily to a laser-based probe tip, in which thermal energy is used to affect treatment to a tissue. However, other types of probes and probe tips can be utilized with aspects of the examples

described herein. In particular, radio frequency emitting probe tips, high-intensity focused ultrasound probe tips, cryogenic probe tips, photodynamic therapy probe tips, and drug injection probe tips can be utilized independently or in conjunction with a light source emitting probe tip, such as the laser-based probes described herein.

A varied level of ablation control is available to a user. With multiple probes inserted into a common sheath, a workstation can independently control each probe within a sheath. Thus, each emission point of the probes can be independently controlled to obtain an arbitrary treatment shape of the tissue. Further, the probes can be independently rotated and longitudinally displaced. By combining the different probes within a common sheath, operation time can be reduced since various steps of the procedure shown in FIGS. **17-19** do not need to be repeated. In particular, various aspects of trajectory planning do not need to be repeated for a number of probes inserted into a common guide sheath.

In light of the descriptions provided herein, a neural ablative laser probe with Joule-Thomson cooling is provided. Further, a laser probe with longitudinally spaced apart emission points is provided, where the probe is rotatable about a longitudinal axis. Additionally, the illustrated longitudinal spaced emission points in the drawings in FIGS. **61-66** can be applied to other probe technologies, including radio frequency (RF) and high-intensity focused ultrasound (HIFU) technologies. HIFU technology, in particular, provides enhanced direction control and greater depth penetration. Further, constructive and destructive interference can be utilized by the plurality of different longitudinal spaced emission points to fine tune a position and depth of energy applied to a tissue.

As shown in FIG. **72**, a probe tip **458** can include electronic emitters **460**. These electronic emitters **460** are longitudinally spaced apart, where the probe tip **458** is rotatable about its longitudinal axis. The longitudinally spaced apart emitters **460** are shown in a regular period. However, the spacing between the electronic emitters **460** can be varied and irregular. The electronic emitters are sonic energy emitters or radio frequency emitters. The probe tip **458** is combinable with the capsule described herein that includes a cooling tube and a thermocouple.

Rotation, intensity, duty cycle, longitudinal positioning, and cooling are controlled by the electronics rack and the workstation. A sequence, such as an algorithm or software encoding, can be executed to cause a probe tip or a plurality of probe tips to execute a particular ablation pattern to affect a predefined treatment scheme to a target tissue area. The ablation pattern can include rotational and/or longitudinal movements.

A probe tip **462**, as shown in FIG. **73**, can include two or more optical fibers **464** and **466**. Optical fiber **464** is illustrated as a diffuse-tip optical fiber, whereas optical fiber **466** is illustrated as a side-fire point emission optical fiber. In this case, the probe tip **462** can provide two separate types of asymmetric ablation. The probe tip **462** also includes a cooling tube and thermocouple or other sensor, in a manner consistent with the other examples, but is not shown. Additionally, other combinations of faceted surfaces or active areas can be combined together, such that any of the laser emission examples described herein can be combined together in a singular probe tip to allow for ablation of a tissue with various types of emission patterns, without requiring a new probe to be inserted into a patient for each ablation pattern. Further, the probe tip **458** shown in FIG. **72** can be included with one or more of the optical fibers shown in FIG. **73**.

As shown in FIG. 74, a probe 468 is illustrated. The probe 468 includes an optical fiber 470 that includes a sheath or clad 472. The sheath or clad 472 is fixed to a capsule 474. In this particular implementation, only the optical fiber 470 extends into the capsule 474. Within the capsule 474, the sheath or clad 472 (and in some implementations, both of a sheath and a clad) are removed from the optical fiber 470, and the optical fiber includes a faceted surface 476. Depending on a structure of the faceted surface 476, the probe 468 can be a diffused-tip probe, a side-tire probe, and/or have a structure that coincides with that illustrated in any of FIGS. 59-70 and 72. In the case of FIG. 72, the optical fiber is replaced with an electrical cable and suitable emitters 460.

In some implementations, the probe 468 can be utilized in the guide sheath 446, where the optical fiber 470 is flexible and allows the optical fiber 470 to bend by contacting a surface 456 and exit through a hole 454. The probe 468 can also be utilized individually, without cooling. A length of the capsule 474 can be approximately 3, 4, 5, 6, 7, 8, 9 or 10 mm, and a diameter of the capsule can be 0.3, 0.4, 0.5, 0.6, 0.7, 0.8, 0.9, 1.0 or 0.5 to 1.0 mm. A non-treatment end of the probe can be fixed to an adapter to connect to a follower to enable rotational and longitudinal control in accordance with the other portions of this disclosure. A diameter of the optical fiber 470 can be 150, 200-800, 300, 400, 500, 600, 700 or 800 micrometers.

A plurality of probe lengths are provided in any of the probe examples described herein based on a degree of longitudinal travel allowed by a follower and a depth of the tissue to be treated. An appropriate probe length can be determined by the interface platform and/or the workstation during a planning stage, or determined during a trajectory planning stage.

Exemplary probe lengths can be indicated on the probes with reference to a probe shaft color, in which white can indicate "extra short" having a ruler reading of 113 mm, yellow can indicate "short" having a ruler reading of 134 mm, green can indicate "medium" having a ruler reading of 155 mm, blue can indicate "long" having a ruler reading of 176 mm, and dark gray can indicate "extra long" having a ruler reading of 197 mm. Different model numberings can also be utilized on the probes to indicate different lengths.

Exemplary lengths of the probe structures are shown in FIGS. 75-77. These figures are drawn to scale and measurements are given in millimeters, unless otherwise indicated. FIG. 75 illustrates the components of the probe shown in FIGS. 3-4. FIGS. 76-77 illustrate the dimensions of an exemplary capsule. An exemplary probe with an outer diameter of 3.3 ± 0.05 mm is shown.

In exemplary implementations, the guide sheath is MRI compatible, and may be introduced through a burr-hole that is created surgically. A sheath with at least one distal opening to be placed in a target area corresponding to a region of interest can be utilized in one implementation. In another implementation, a sheath with at least one proximal opening can be provided for the delivery of other or a plurality of devices. In some aspects, the sheath may be air-tight for a neurosurgery operation. The sheath may also include a through lumen to allow other devices to be delivered therethrough. The sheath may include a walled structure to physically or mechanically support other devices inserted therein. A sheath may also be delivered with an introducer and a wire. A sheath in accordance with one or more of these aspects can allow for multiple accesses to a treatment site while avoiding undesired interruption of a meninges layer. A sheath in accordance with one

or more of these aspects can allow for an expanded treatment space through multiple apparatuses with minimal invasive access.

V. Head Coil And Stabilization System

An exemplary head coil and stabilization system that can be utilized in accordance with the various aspects presented in this disclosure is described in WO 2012/137179, filed Apr. 5, 2012, the entirety of which is incorporated herein by reference.

FIG. 2 illustrates a patient inserted into a bore of an MRI. The patient's head is fixed to a head fixation ring by fixation pins. The ring is received in a ring mount of a platform. The platform extends, in a direction away from the bore, providing a head coil support. After a miniframe is installed onto the patient's head, and the patient's head is fixed to the head fixation ring, an MRI coil is coupled to the fixation ring and the coil support. Further, as shown in FIG. 2, the coil support includes receiving holes for attaching the interface platform thereto.

FIG. 78 illustrates a platform 500 including a plurality of handles 502. After a patient is sedated, and the trajectory planning procedure is completed, a miniframe and/or fixation ring is attached to the patient's head. The fixation ring can be secured to the ring mount 504 in, e.g., an operating room in which the trajectory planning procedure is conducted. The patient can then be wheeled to an MRI room, where operators/assistants can utilize the handles to move the fixated patient from, e.g., a wheeled operating table to an MRI table. A head coil is fixed to the fixation ring and/or the head coil support 506 in the operating room on the operating table or in the MRI room on the MRI table. An interface platform is inserted into the receiving holes 508, which is illustrated in FIG. 6.

As shown in FIGS. 78-79, the ring mount 504 includes a channel 510, in which a fixation ring rests. The fixation ring is locked into the ring mount 504 via knobs 512, which are provided at distal ends of the ring mount 504. FIGS. 78-79 illustrate alternate perspective views of the ring mount 504.

The ring mount 504 includes attachment mounts 514. The attachment mounts 514 can be utilized in a trajectory planning stage to mount a reference array, such as, e.g., a reference guide of an image-guided surgery system. In particular, a tracking instrument is attached to the attachment mounts 514 to locate the head fixation ring 516 (and therefore the other components of the stabilization system, including the head coil etc.) in rendered space. A convention reference array utilized in image-guided surgery can be utilized with the attachment mounts 514.

FIG. 80 illustrates a head fixation ring 516 fixed to a patient's head 518. A miniframe, probe follower, and probe are attached to the patient's head, and an interface platform is coupled to the platform 500 and wired to the active components. A head coil 520 is fixed to the head fixation ring 516, and includes, generally, two halves. A first half 522 has a half-cylindrical shape and is substantially continuous. A second half 524 has a generally half-cylindrical shape, but includes a slot 526, which extends in a longitudinal direction of the patient. A bent portion 528 of the second half 524 of the head coil 520 bends towards a longitudinal axis of the patient in the direction towards the interface platform, in the direction away from the patient. As a result, a continuous coil can be provided, which allows for a trajectory to be aligned at or near a side to forehead region of the patient's head. In the event that a side trajectory (i.e., entry into a side of the patient's head) or a top-of-head trajectory is planned, a head coil that does not include a bent portion, but merely includes a slot that coin-

cides with a cylindrical structure, can be utilized. These various head coils can be interchanged with the first half **522** of the head coil **520**.

The first half **522** of the head coil **520** also includes a plug connector **530** that is coupled to a cable **532**, which is in turn connected to the MRI system. This cable **532** energizes the head coil **520** and/or transmits data signals. The length of the cable **532** can be adjusted to accommodate a particular arrangement of head coils and other structures provided with the MRI.

FIG. **81** illustrates the head fixation ring **516** including a plurality, such as two, fixation posts **534**. These posts **534** each include a series of holes, each of which can engage a fixation screw **536**, which presses portions of the patient's skull above and in front of the patient's temples back against a backrest **538**. The head fixation ring **516** includes a plurality of holes **540** that are provided to engage a locking pin (not shown) from the knobs **512**. The head fixation ring **516** can rotate within the channel of the ring mount **504**, but is rotationally locked by engaging the knobs **512** with one of the holes **540**.

FIG. **82** illustrates an exemplary second half **542** of the head coil **520**. The second half **542** includes a slot **526**, and is suited for access in the direction of the bold arrows shown in FIG. **82**. The second half **542** includes connectors **544** that provide alignment and electrical connections with corresponding connections on the first half **522** of the head coil **520**. FIG. **83** illustrates another view of the second half **524** of the head coil **520**, where access to a patient's head in the direction of the bold arrows is provided. As shown herein, the second half **524** also includes connectors **544**.

In light of the descriptions provided herein, the head coil **520** and the head fixation ring **516** are rotated to suit a particular trajectory, and are locked into place. The interchangeability of the second halves of the head coil allows for flexibility in trajectory planning, and accommodates the physical presence of a miniframe, a follower, and a probe. Either of the second halves **524** and **542** allow for a rotatable portal, such as the slot **526**. In particular, the slot **526** is rotatable about a longitudinal/patient axis, and can be fixed into place via the head fixation ring **516**. The slot **526** allows for side or angled points of entry into a patient's skull. These points of entry can be referred to as radial points of entry, and the structures described herein allow for radial points of entry along an entire crown line of a patient, while fixating the patient's head. The bent portion **528** of the second half **524** provides a rotatable portal that allows midpoints between a side of a patient's head and a top of the patient's head to be accessed directly, while still maintaining continuity with respect to the electromagnetic properties of the coil.

Other coils can be attached to the head fixation ring **516** or to another type of ring that is fastened to the platform **500**. The platform **500** can be adjusted to adapt and connect to various different MRI tables, such as different MRI tables provided with different MRI machines.

VI. Visualization And Control

FIG. **1** illustrates a control workstation provided in an MRI control room, as well as an electronics rack in an MRI equipment room. The electronics rack is coupled to an interface platform by various electronic, optical and cooling fluid cables. The electronics rack is also connected to the control workstation by, for example, network cabling or other data transfer cables. Although not shown, the electronics rack and the control workstation can be coupled together by a network, such as an Ethernet network. In another implementation,

electronic data cables can be routed directly from the interface platform to the control workstation, without use of any intervening devices.

A. Planning

i. Plan Register

An operator can operate the workstation to initialize software executed on the workstation to provide a control terminal and graphic user interface for creating a plan, which defines an organization of appropriate information for the treatment of a particular tissue. To initiate and create a plan, the user operates the workstation to execute a graphic user interface, such as graphic user interface (GUI) **600**, shown in FIG. **84**. The GUI **600** includes a selectable area (herein referred to as an area, button or region) **602** for selecting a particular MRI system, such as a brand/model of an MRI. An area **604** is provided to include brief instructions and/or comments to an operator, and a start area **606** is provided to initiate the start of a plan.

FIG. **85** illustrates a screenshot of a registration of the plan. In this screenshot, the GUI **600** includes an information area **608**, which indicates that all image sets are registered to a single master series. Adjustments to images and images sets can be made via the GUI **600**. For example, a blend area **610** is provided for adjusting a blending ratio. Further, an area **612** is provided for making other adjustments to the images, including magnification, panning, contrast, and others. Markers can also be included in the images to identify a particular tissue of interest. Further, in this screen, images can be loaded from the various data sources, including a network storage unit or a local portable storage unit, such as a USB drive. As shown in FIG. **85**, multiple images can be arranged in a thumbnail view, which allows a particular thumbnail to be selected and shown in one of a plurality of larger views.

FIG. **86** illustrates registration amongst the plurality of images. In region **614**, various selectable areas are included, including auto-registration, registration tools and registration verification. Auto-registration performs a best-fit analysis of two anatomical data sets (e.g., images) based on predetermined thresholds within an anatomy. If the auto-registration is deemed inaccurate by an operator, or if a manual registration is desired, the rotate and pan selectable areas of the registration tools can be operated to adjust the registration. The blend selectable area allows for an accuracy of the registration to be checked by a user, by blending a selected data set into or out of view with the master series. This tool is used to verify the registration accuracy of each image set registered to the master series. Once accurately registered and verified by the operator, the operator can indicate that the registration has been verified by selecting the verify registration area of the registration verification portion. After the images have been registered, a volume can be planned.

ii. Plan Volumes

FIG. **87** illustrates a volume planning screen of the GUI **600**. In this screen, contours can be inputted via the selectable areas including region **616**. With this interface, an operator can define all regions of interest using contour tools. Parallel contours can be drawn on any plane. Perpendicular contours can be drawn on sagittal and coronal views. This interface allows an operator to generate volumes or intended treatment areas, also known as regions of interest (ROIs), within the data set in different pre-set colors. An ROI can be defined here using appropriate contour tools provided by the GUI **600**. For treatment of a tissue, the operator creates at least one ROI over an intended treatment area. The planned volumes portion is accessible by selecting an appropriate selectable area, such as area **618** to select a volumes task.

FIG. 88 illustrates an interactive method of generating a two-dimensional contour. An interactively segmented contour can be selected by selecting area 620 of the GUI 600. This outlines a desired region and then generates a volume from the contours. Different contours are drawn in the sagittal or coronal views, and these contours are computed, by the workstation, to generate a volume.

FIG. 89 illustrates how the contour can be adjusted by using an editing command, such as a push command, via selectable area 622. Since an intended area for treatment of a tissue is generally not symmetrical, the push command allows for a pushing action to be implemented on the contour shown in the various views of the GUI 600. In particular, a contour at an intended location can be created in each of various orthogonal views. This contour may initially resemble a geometric shape, such as a circle or an oval. Then, this or other contours can be edited as required by the operator with the push tool. By operating a mouse or other input instrument at the workstation, the operator can push the boundaries of a contour with, for example, the white circle shown in FIG. 89 to achieve a desired shape. The size of the white circle can be changed by toggling a button on the mouse to accommodate larger or smaller manipulations. For example, while activating a left or right click button of a mouse, the size of the push tool can be changed by operating a wheel of the mouse. Contour lines can also be deleted by checking a clear all button on the GUI 600, and a shape of the push tool can also be changed from a circle to, for example, an oval, a square or a triangle. Other geometric metric shapes can also be utilized.

After the contours have been defined in the orthogonal views, a volume can be generated by the workstation by selecting the area 624 shown in FIG. 89. This volume, as well as any other volumes created in accordance with the description provided herein, can be named, edited, deleted, renamed, and saved in a storage medium, such as a hard disk or portable drive, of the workstation.

iii. Plan Trajectory

After a volume has been identified, or several volumes have been identified, a trajectory for affecting a treatment to the volume(s) can be planned. Trajectory planning is shown in FIG. 90. Here, the volume is encircled in several orthogonal views of the tissue, according to a saved or accessed volume plan. A probe trajectory-coronal view, a probe trajectory-sagittal view, and a probe's eye view are shown in FIG. 90. A trajectory 626 is planned for treating the encircled volume. White circles indicate insertion and maximum depth markings for the probe. This planning is intended to define an initial trajectory while in a planning phase. The final trajectory used for actual treatment can be modified later, if necessary. A new trajectory is defined by manipulating "grab-handles" (which are defined as the two white circles within the views). The point of deepest penetration (PDP) is defined by the workstation as a centroid of the deepest grab-handle to the deepest point in the brain allowable for probe insertion. This screen can also provide a 3D surface rendering, as shown in the lower right of the screen of FIG. 90.

Once a trajectory has been defined, a save command can be issued to save the trajectory. Once the trajectory is saved, a new trajectory can be generated for the same volume or for another volume. The trajectories can be saved so as to correspond with a particular volume. This correspondence can be saved by the workstation in an association file. For example, during the treatment stage, a particular volume can be identified, and the workstation can provide associated trajectories for that particular volume.

The various trajectories and volumes defined in accordance with the descriptions provided herein can be saved as a plan,

as a file in the workstation. The file can be saved to a local or remote storage device. A saved plan can then be accessed later. For example, a plan can be accessed during a treatment planning stage, and the plan can be part of an executed sequence by the workstation to enable a continuous process of treating a plurality of volumes or a plurality of positions by the workstation without requiring further planning or setup input by an operator.

B. Pre-Treatment

i. Preparation

After a plan has been generated, a patient is prepared and the appropriate components are collected for conducting a treatment. In particular, a mini frame and a delivery probe are acquired, in accordance with the disclosures provided herein. Various drill bits are acquired for drilling a proper bore hole size into the patient's skull. Additionally, an image guided surgery alignment adapter is acquired. The particular image guided surgery alignment adapter is generally specific to the particular operating room and/or hospital and is mounted to, e.g., a stabilization system affixed to the patient.

At this time, operating systems of the electronics rack and the workstation can be verified. In particular, new medical grade carbon dioxide tanks can be installed into the electronics rack to be used for cooling, and power to the workstation can be verified. The patient is anesthetized according to anesthetic requirements for the procedure being performed. Further, the patient can be provided with earplugs in both ears in preparation for the MRI scanning, and a medically tested and MRI compatible temperature probe can be inserted into the nasopharynx of the patient for accurate temperature readings throughout the procedure.

ii. Head Fixation

Post-anesthesia, the patient's head is fixated within an MRI compatible head fixation device using MRI compatible fixation pins. An image guided navigation system is registered based off of a pre-operative scan. Once the image guided navigation system is accurately registered, an entry point is defined on the anatomy and the incision plan is made. An exemplary head fixation mechanism is described in Section V.

After the head fixation system has been successfully attached, proper sterile draping is applied. Further, since a miniframe and an interface platform need to operate in conjunction with the other components, care should be taken to ensure that the sterile draping does not interfere with any such components or other components utilized in the planned treatment. At this time, pilot holes can also be drilled into the patient, should the patient have a very dense/hard skull or if the patient has a cranial plating system.

iii. Miniframe

The miniframe is then mounted to the patient. An exemplary miniframe is described in Section II. At this time, the miniframe can be used as a drill guide. Otherwise, a different guide can be used as a drill guide.

Also, for each foot of the miniframe, the foot should be pressed firmly into the scalp at a respectively marked location until all spikes of the feet are fully seated on the skull surface. By holding a foot in place, the screws should be engaged with a sterile screwdriver. The screws should be alternately advanced until all screws are fully seated. The stability of the feet attachment should be verified before proceeding. A template linkage, which maintains a predefined displacement between the feet of the miniframe, can then be removed. The miniframe can be aligned using the image guided navigation system. In particular, as shown in FIG. 91, an image guided navigation system pointer probe 628 is shown inserted into an alignment adapter 630 of the miniframe. As such, the image guided navigation system can visualize the trajectory into the

anatomy on a pre-operative scan/screen. Once alignment is secured and the miniframe is locked into position, the pointer probe 628 can be removed and replaced with an appropriate drill. A depth to a predetermined target, i.e., the plan volume, can be determined via a biopsy needle or via the depth pre-defined in the image trajectory planning.

After the drilling has been completed, an MRI trajectory wand can be inserted into the miniframe. The patient can then be prepped and draped for insertion into the bore of the MRI.

C. Treatment

i. Scan & Register

After the patient is loaded into the bore of the MRI, and the various corresponding components are attached and connected, in accordance with the other disclosures provided herein, the patient is scanned to detect the trajectory wand placed in the miniframe. An exemplary screenshot of an image including the trajectory wand is shown in FIG. 92 as item 632. Also shown in FIG. 92 are various orthogonal views of the patient's skull, together with a three-dimensional rendering. Based on these various views, an operator can verify an alignment of the trajectory wand 632 with the previously planned trajectory. Additionally, a new trajectory can be created if necessary.

Once the trajectory has been aligned via the trajectory wand and saved within the planned trajectory section of the GUI, a detected fiducial marker within the miniframe is defined to provide a depth setting and a directionality for a probe within the GUI in accordance with the screen shown in FIG. 93. Fiducial markers can be auto-detected by selecting an auto-detect button 634 in the GUI. If the auto-detection does not result in detecting the fiducial markers for the miniframe, the fiducial marker can be manually set via the region of buttons 636 shown in FIG. 93. As a result, two circles or other markers 638 are indicated in the GUI as identifying the miniframe. Further, since the trajectory wand may still be inserted into the miniframe, the trajectory wand image 632 may still be visible within the image, and proper alignment amongst the various components can be verified within the GUI.

ii. Define ROI and Trajectories

A previously planned plan, i.e., ROIs and trajectories, is accessed via the workstation and loaded into the GUI. Consistent with the disclosures provided herein, a plan can be modified or ROIs and/or trajectories can be added to or deleted from a plan. Data management (i.e., saving/modification thereof) can be provided via a local storage unit of the workstation or via a portable storage unit (such as a USB drive that is particular to the patient).

iii. Probe Insertion

After a region of interest has been defined and image trajectories have been registered in the GUI and saved to the workstation, a pre-insertion point is defined in the GUI for probe insertion. A manual self-test is then conducted to verify that the system is ready for treatment. The pre-insertion point is defined by moving a probe tip 640, as shown in FIG. 94, within the anatomy to the point that the operator wants to see the probe upon initial insertion into the desired area. Once this probe tip 640 is moved to the desired position, another manual self-test is performed. This test is started by clicking on a corresponding start button of the GUI. At this time, the probe tip 640 shown in FIG. 94 is a rendered probe tip, which does not correspond to a physical probe tip, at least yet. A last step in the self-test procedure is manually inserting in the probe. Once the probe is physically inserted into the patient, the GUI is operated to register or match the hardware of the probe with the probe tip rendered in the GUI.

iv. Software to Hardware Match

When scanned by the MRI, the physical probe inserted into the patient is viewed from the workstation as a probe artifact within the image. This probe artifact is registered and coincides with the probe tip 640 shown in FIG. 94. Scan plane parameters can be selected to coincide with the position of the probe inserted into the patient. Once a new image from these parameters is loaded into the GUI, an alignment of the probe artifact can be registered with the rendered probe by adjusting grab bars of the rendered probe to match perfectly with the alignment of the probe artifact, as shown by grab bars 642 of FIG. 95. Once the trajectory is perfectly aligned, a trajectory can be confirmed by selecting an appropriate box in the GUI. Additionally, as shown in FIG. 95, a depth stop, linear position and rotary angle of the probe can be tracked and/or set in area 644 of the GUI. The linear position and rotary angle of the probe is determined by the predefined relationships between the probe, the follower and the miniframe. These predefined relationships are spatial relationships that are utilized in image guided navigation systems and verified in MRI images.

v. Treatment

Once the trajectory is confirmed and the physical probe inserted into the patient has been registered with the GUI to coincide with the rendered probe image, a depth and direction of the probe is set to a first desired location to initiate treatment. Prior to treatment, and after registration of the patient has been completed, a real-time transfer from the MRI is established. This real-time transfer is established by issuing appropriate commands via the workstation to send images in real-time from the MRI to the workstation. At this time, the workstation receives real-time imagery from the MRI.

In receiving real-time images, since the actual probe position (i.e., the physical position of the probe inside the patient) is registered in the GUI and the workstation, the actual probe can be indicated by a color position. As shown in FIG. 96, this colored position is a red graphic. A target position of the probe can be rendered by a blue graphic, as further shown in FIG. 96. These colors and indications can coincide with the labeling and colors utilized in the probe information area 644 of FIG. 95. As shown in FIG. 96, target and actual longitudinal positions and rotary angle positions can be shown by corresponding red and blue graphics.

An adjustment of a linear or rotary position of the probe can be made by selecting the corresponding portion of region 644 of FIG. 95, and entering appropriate values through, for example, a keyboard. The target renderings of at least FIGS. 95-97 can also be selected by a cursor or mouse input by clicking thereon, and dragging the rendering into an intended position. In response, the workstation can transmit corresponding signals to the interface platform, which in turn can rotate corresponding knobs on a commander, and consequently affect movement of linear and rotary positions of the probe via the follower. This can all be done in real-time, where the workstation issues corresponding instructions and commands immediately in response to an operator's interface with the GUI. On the other hand, an execute or OK button can be provided with the GUI, to delay actuation of the probe to the intended position until the OK button is selected by the operator. Further, the GUI can include parameters indicating thresholds for linear and/or rotary travel, such that when an operator issues a command that is outside the threshold range, a warning is provided and the probe is not moved.

Moreover, the grabbing and repositioning of the probe can be stored as a sequence, which includes a plurality of positions and alignments of the probe, which correspond to a series of treatment positions for treating various portions of

the ROI. This sequence can be executed in an automated or an assisted fashion via the workstation. In particular, in one implementation, an operator saves a sequence including a plurality of different probe positions, and the workstation transmits corresponding instructions to effect probe movement after predefined treatment levels are reached in each position. Treatment can then proceed to a next treatment, where the operator merely supervises progress or maintains activation via a foot pedal, the release of which would pause or stop probe activation/treatment. In this case, the workstation would effect proper probe and tissue cooling between each repositioning, and one or more ROIs can be treated continuously without interruption.

In another implementation, the workstation calculates a minimum number of positions or a minimum amount of time necessary to effect treatment of the ROI(s). Here, the workstation estimates an amount of time necessary to effect treatment of an ROI at a plurality of different positions, and compares the various positions with their respective amount of treatment times. Then, the workstation calculates a combination of positions and corresponding treatment times that result in a shortest operation period. The resulting combination of positions and treatment times can be displayed to the operator, either as a list of steps or in a preview. The preview can include a visual rendering of how the total procedure is expected to progress. This workstation-calculated sequence can be verified by the operator or particular portions of the sequence can be modified by the operator. The workstation-calculated sequence is performed based on an expected output of a particular probe, and can compare different types of probes and combinations of probes in a particular sequence. For instance, in one implementation, the workstation calculates steps in a sequence that starts with a symmetric treatment by a probe, and then calculates steps with an asymmetric treatment by another probe.

Treatment, in accordance with the workstation-calculated (and/or operator modified/confirmed) sequence, proceeds where the operator may merely supervise progress or maintains activation of one or more of the probes by, e.g., a foot pedal (the release of which would pause or stop probe activation/treatment). In this case, the workstation can effect proper probe and tissue cooling between each repositioning, and one or more ROIs can be treated continuously without interruption.

Linear and rotary travel (e.g., repositioning) of the probe is conducted while the MRI is in operation, and an operator is not present in the MRI scan room. Parameters are entered into the GUI or accessed by the workstation for a scan plane for a thermometry sequence prior to initiating a thermometry scan. At least FIGS. 96 and 97 illustrate exemplary scan planes 646, and an exemplary view of these scan planes 646. These scan planes are continuously scanned in sequence by the MRI and sent to the workstation in real-time. Lower images 648 and 650 of FIG. 97 are also imaged in sequence and sent to the workstation in real-time.

When the MRI images begin arriving from the MRI, an initialization phase of the workstation and GUI computes a noise mask and allows for reference point selection. The GUI receives data from the MRI and updates itself with a solid colored overlay indicating pixels that are a part of the mask, as shown in FIG. 97. The mask, in one implementation, is a circular region of six centimeters in diameter, which surrounds the probe and which represents a sub region of the MRI images being acquired. Any data, for thermometry purposes, outside of this region is ignored. The MRI data within the mask is analyzed for each measurement. Pixel locations which show excessive phase noise will not be used for tem-

perature measurement and are cleared or rendered transparent in the mask overlay. These are referred to as masked pixels. An example is shown in FIG. 97.

As MRI acquisition continues, the operator selects a minimum of 8 reference points surrounding the treatment area within each view. Reference point selection is shown by example in FIG. 98. More or less reference points can be selected, such as 1, 2, 3, 4, 5, 6, 7, 9, 10 or more. However, 8 reference points is an exemplary suitable number. Further, the workstation can auto-select reference points, which are then confirmed by an operator. The workstation auto-selects reference points by selecting a plurality of points that are separated from each other, the ROI and/or masked pixels by predefined thresholds. The operator can also adjust reference points after the workstation auto-selects the reference points. The reference points indicate regions of the brain that are not intended to be heated, and are utilized in establishing a baseline temperature. In addition to the reference points, a minimum of eight measurements is acquired before an operator proceeds to temperature and thermal dosage or damage monitoring.

Once the reference points have been selected and a sufficient number of MRI measurements (e.g., eight) have been acquired, treatment monitoring can start by selecting a start temperature monitoring button 652 of the GUI, as shown in FIG. 98. Prior to proceeding with treatment, a current body temperature of the patient is entered into the workstation via the GUI, as well as a current probe temperature. The current probe temperature is retrievable via the workstation through a thermocouple connection within the capsule of the probe, which is coupled to the workstation via the interface platform, the electronics rack, and appropriate wiring connected to the workstation.

After inputting a baseline temperature, the color overlay of the masked region can be changed to a corresponding color on the color temperature map. FIG. 99 illustrates the mask region as a color which corresponds to a 37° C. baseline temperature. Other baseline temperatures within a range of 36-38° C. can also be utilized. This color can be green. At this time, probe cooling commences, which can cause the pixels in the vicinity of the probe to begin to shift from green into a blue region, indicating the tissue is being cooled. This verifies that the cooling in the probe is operating under normal conditions. An operator can stop the procedure to inspect and verify equipment if cooling does not appear to be operating as intended. Further, the workstation can detect an error and output a warning or discontinue treatment if a calculated amount of cooling does not result in an intended detected cooling within the ROI.

As illustrated in FIG. 99, an interface 654 within the GUI can be selected to change a mode of the probe from a standby mode to a ready mode, in which a foot pedal attached to the workstation is active to actuate a laser of the probe when the mode is switched to ready. If the standby mode is active, then the foot pedal does not control laser output or any probe activation. If probe cooling is not operating within set conditions or another problem is detected, then the GUI and the workstation inhibits an operator's selection of the ready mode for the probe. Lazing commences upon verification by the workstation and the GUI that settings are appropriate and conditions are within the predetermined thresholds. As illustrated in FIG. 100, treatment results in the GUI are shown by the GUI creating an isoline or contour line 656, which indicates a specified threshold of thermal dosage. The isoline or contour line 656 is illustrated contemporaneously, in real-time, in various views, including several (e.g., three) axial planar views, a coronal view and a sagittal view. The GUI and

the workstation can halt treatment by the probe when the isoline or contour 656 coincides with a boundary of the region of interest that was planned in the trajectory and volume planning procedures, or when the isoline or the contour 656 satisfies a predetermined step within a sequence. Once the probe is stopped, the workstation and GUI can cool the ROI back down to the baseline temperature, initiate rotation and/or longitudinal repositioning of the probe and commence treatment at a different portion of the tissue. This procedure can be repeated until a plan volume has been detected as being treated to a sufficient level, by means of manual operation, a semi-automated operation or an automated operation.

During the entire procedure discussed above, the operator maintains activation of the foot pedal. Release of the foot pedal stops or pauses treatment. The treatment can be resumed upon reactivation of the pedal.

The various treatment trajectories for treating one or more volumes are stored in a workstation as individual sequences, which can be executed by the workstation automatically, without specifically requiring operator input to proceed from one sequence to a next sequence, or from one part of a sequence to a next sequence. A changeover between sequences or portions thereof can include at least one of rotational alignment change, longitudinal position change, laser fiber selection, probe tip selection, energy output, and duty cycle of energy output. In particular, when more than one probe is utilized contemporaneously, varying the probes in accordance with Section IV can be utilized in these sequences, and can be interchanged continuously without interruption of the operation of the MRI or the real time transfer of data from the MRI to the workstation.

vi. Noise Masking, Reference Points and Thermal Damage Monitoring

Further aspects of selecting reference points, masking noise and monitoring thermal damage are described herein.

Aspects of this disclosure encompass a system, method, devices, circuits and algorithms for monitoring the treatment of tissues, such as tumors, that include a process or algorithm for correcting incoming MRI data in order to compute accurate changes in temperature over time. MRI systems suffer from "phase drift," which may appear as a cyclical fluctuation of "phase data" that would otherwise remain constant if no other factors were present to influence the phase data. Factors that may influence phase data and cause such fluctuation may include, for example, tissue heating or motion. The selection of "reference points" may be used to compensate for phase drift in order to provide accurate temperature and thermal damage values to a user.

Magnetic resonance data includes complex numbers where both a magnitude and phase component exists. The magnitude data may be used to illustrate the "magnitude image," the most common data form used to visualize MR data. The magnitude image may provide, for example, a typical gray-scale image of the brain showing contrast between different structures. The second set of data that is acquired is known as "phase data," which is representative of a phase of the image being displayed. Most MRI applications do not have a use for phase data, and merely discard this type of data. However, certain applications, such as phase contrast angiography, MR elastography and the temperature monitoring application described herein, may utilize the phase data. One reason for its value is that temperature is sensitive to the water proton chemical shift which is determined by the proton resonant frequency. This can be quantified from the phase component of the MR complex data.

Each pixel in a phase image has a value, particularly, an angle expressed in radians. Generally speaking, as long as the

temperature of the tissue being monitored remains substantially constant, the phase values associated with the tissue should also remain substantially constant. For example, if an image of the brain is viewed every few seconds, such as 3, 4, 5, 6, 7, 9, 10 or more seconds (such as 8) for 2, 3, 4, 5, 6, 7, 8, 9, 10 or more minutes (such as 5), and then a specific pixel in the image is selected and plotted over time, ideally the phase number value for the selected pixel should be the same throughout the entire duration so long as the temperature remained substantially constant. Furthermore, if the temperature of the brain was raised or lowered, the phase number value should also be adjusted accordingly in response to the temperature change. Temperature is inversely proportional to phase change. For example, if the temperature of the brain was lowered, then there would be a corresponding increase in the phase number value, and vice versa.

One problem addressed herein results from the fact that MRI systems are not perfect. Such systems actually force a natural fluctuation of phase over time due to fluctuations in the magnetic field. Therefore, even when no heating is being applied to the tissue, the phase value of a selected point on an image may fluctuate over a period of time. For instance, the graph of phase values over time may appear sinusoidal. This type of fluctuation is problematic for temperature mapping because if the system does not correct for the fluctuation, the user may incorrectly think that the temperature is increasing or decreasing when in actuality it is substantially constant.

For example, until heat is applied to a brain during a treatment procedure, the brain tissue should remain at a baseline temperature of. Therefore, when phase values are plotted over time, the fact that the phase value fluctuates may mean that there is, for example, a drift in the magnet in the MRI. Workstations are useful for tracking this drift. As will be explained in further detail to follow, reference points may be selected in tissue areas that a user knows will remain at the baseline temperature prior to any heat treatment. Thus, by looking at the pattern of the drift in the reference points, the workstation or an MRI control workstation extrapolates the drift pattern to all of the areas in the image in order to compensate subsequently received images. As a result, the phase drift can be accounted for (as a constant) and removed so that any fluctuation that an operator observes is actually related to temperature, and not extraneous factors.

In one example, eight reference points may be selected within each of a plurality of predefined treatment slices of brain tissue and used to compensate for phase drift during the treatment. These reference points preferably reside within native brain tissue but are far enough away from the position of a treatment probe such that the tissue surrounding the points will not experience any substantial heating. Preferably, treatment should not be allowed to commence until the reference points are selected and confirmed by the operator. In one exemplary process, five of the eight reference points may be the "primary" points that are initially used in a masking phase, while the remaining three reference points may be used as "buffers" in case some of the primary points are dropped due to poor signal quality as the MR acquisition continues.

In one example, the user may select the reference points in a generally circular pattern surrounding the targeted treatment area. Selecting reference points surrounding the treatment area may provide a substantially uniform correction around the treatment area.

A two stage noise masking phase can be used to assist an operator in selecting reference points. In particular, when MRI thermometry data (both phase and magnitude) is validated and accepted by the workstation, a mask may be com-

puted to hide those pixels which are considered to be “noisy.” Until the operator selects to proceed in the workflow to view temperature data, the MRI raw data may be shown as a binary image of pixels that pass the noise masking stage and those that do not pass the noise masking stage. For example, the pixels that pass the noise masking stage may be made opaque, while the pixels that do not pass the noise masking stage may be made transparent. Other methods of distinguishing the pixels that pass the noise masking stage from those that do not pass the noise masking stage are also possible.

FIG. 101 illustrates a sequence of processes performed via operator interaction and by data processing by, e.g., a workstation. The sequence is set forth in three stages in a time-wise sequence based on an MR measurement number. This sequence is exemplary and includes various computations performed by the workstation.

With reference to FIG. 101, the first stage of noise masking (Stage 1) may simply analyze the quality of the incoming phase data, applying a threshold to formulate a masked image. During this process, the operator may select reference points in each of a plurality of views. Points that do not fall within the noise mask may be deleted. Once the minimum number of reference points has been selected, the process may then continue to a Stage 2 noise mask to compute a phase drift compensated temperature difference. Stage 1 may be immediately skipped if the reference points already exist prior to MRI data arriving.

In Stage 2, the reference points selected in Stage 1 may be “validated.” The reference points are used to compute a temperature difference at every location within the Stage 1 masked region. A temperature threshold can then be applied. Pixels whose temperature difference exceeds the threshold can be removed or masked, indicating to the operator the stability of the temperature mapping in the treatment area prior to treatment. The operator can continue to select additional reference points or delete existing reference points in order to produce a stable temperature map.

More particularly, two parallel actions are occurring as soon as the MRI system begins to take measurements. First, the operator may begin selecting reference points in the Stage 1 noise masking process in order to begin the reference point correction sequence. However, parallel to the Stage 1 noise masking process an optional “filtering” sequence of steps that filters out noisy points may be performed. In particular, the filtering sequence may begin by generating a default mask wherein all of the overlay pixels are opaque. The system may be designed such that the masked raw phase data may be displayed, for example, so that opaque pixels represent stable phase locations. Thus, at the most basic level the filtering sequence may involve comparing a first image to a second image and masking the pixels when unreliable data exceeds some threshold.

Within Stage 1, the operator begins selecting reference points based on the masked phase data resulting from the filtering sequence previously described. As briefly mentioned above, reference points are points on an MRI image that may be selected by the operator, such as by pointing and “clicking” a mouse cursor at a desired image location. For example, when an MRI system is running it typically may send data about every eight seconds updating the image. In overlaying the MRI image there may be another image that may ultimately become the temperature mask. The temperature mask may be made transparent or opaque through the use of a transparency control. Within the overlay, the operator selects points that are sufficiently far from the area that will be heated during treatment. These points are the reference points, and they all should fall within the brain.

The reference points are indicators of image or phase drift in the MRI. Because a certain amount of image or phase drift occurs naturally, once this natural image or phase drift in the MRI is determined, all of the subsequent phase data for the image may be compensated. The reference points may be selected either subjectively by the operator or automatically by reference point selection software. Whether the selection is performed manually or automatically, it will involve numerous factors including determining the location of the brain, segmenting the brain from the skull and other anatomical parts, and the like. If the minimum number of reference points has been selected, then the operator is free to move on to Stage 2.

Any number of reference points may be used in accordance with the descriptions provided herein. A single reference point may provide only a single point correction and a substantially planar fit providing a single correction value to all pixels within the image. Two or three reference points can provide a planar fit which may not describe the variable phase drift in the image correctly. Thus, when a planar fit is used, there is no “averaging” component. However, with more reference points, the points can be extrapolated to the entire image, providing for a polynomial surface fit in 3-D space. Thus, using a polynomial fit through the selected points is preferable because it allows for suitable correction throughout the entire image. In some implementations, the polynomial fit is superior to a planar fit generated by 1, 2 or 3 reference points. Fitting a polynomial surface to the selected points can create a correction throughout the entire treatment area without actually having to pick points at every location.

Further, although as few as one reference point may be sufficient for a basic planar fit, a larger number may be preferable because the operator may unintentionally pick one or more “unusable” points. This can occur when the signal intensity at the reference point location drops too low indicating poor signal and thus an unreliable phase value. Although eight reference points are described, any number of reference points having any number of extra “buffers” may be used without departing from the intended scope of the descriptions provided herein.

Once the minimum number of reference points is selected in Stage 1, the process continues to Stage 2 where the reference points may be used to correct for the phase drift. Until the operator transitions to the Stage 3 temperature monitoring stage, the operator remains in the masking stage and temperature is not yet being shown. In particular, during this masking stage the system assumes that the brain tissue is at a stable baseline temperature. As a result, all of the pixels displayed in the treatment area on the screen should be at approximately the same, constant temperature. The temperature of each pixel is computed and compared against a threshold to filter those regions where excessive temperature changes are occurring based on the currently selected reference points. Thus, the operator should be careful so as to select the reference points in a substantially homogenous brain tissue because too many pixels can be masked out due to reference point locations to correct for drift.

The result of the Stage 2 computations may be a phase map comprising a polynomial surface. More particularly, when computing the polynomial surface in accordance with the descriptions provided herein, the algorithm should include each of the reference points selected by the operator. The algorithm then functions to create a “surface” that represents the “best fit” through all of the selected points, or alternatively close to all of the selected points. As will be appreciated by those skilled in the art, when four or more reference points are selected, a polynomial surface fit should be used because it

may be mathematically impossible to fit a planar surface through four reference points. Utilizing a polynomial surface fit is preferable when MRI phase drift is not linear. In one example, there may be slightly more phase drift at the top of the brain and slightly less phase drift at the bottom of the brain. Thus, the correction across the entire image preferably utilizes a polynomial fit rather than a planar fit.

After the corrected phase has been computed, the method proceeds to compute a drift compensated phase difference based upon the current corrected phase and a baseline phase that is stored in memory, such as an electronic memory of the workstation. Next, the drift compensated phase difference is then multiplied by a constant (a PRF factor), which gives us a temperature change in degrees Celsius. The baseline temperature is added to the temperature change to arrive at a current absolute temperature value. The baseline temperature may generally be about 37° C., which is the "normal" temperature of brain tissue prior to any heating or cooling. Other temperatures can be set, including 35° C., 36° C., 38° C., 39° C. or any fractional temperatures therebetween.

In Stage 2, temperature is not yet being displayed, but rather is rendered just as a mask. Therefore, what is being displayed in Stage 2 are pixels representing computed temperatures that fall within a predefined tolerance. If the computed temperatures fall within the tolerance, then the corresponding pixels are not masked out. However, if a computed temperature change is outside of the tolerance, then the corresponding pixel is masked out. This step in the process may be performed to illustrate how stable the data is so that prior to actually transitioning to the treatment mode (Stage 3), the operator may visualize the overlay mask on the image. If the operator observes that too many pixels have dropped out, then this serves as an indication that there may be a problem with the phase MRI. For instance, the MRI may not be functioning properly or there may be something wrong with the acquisition of the data that is creating too much variation in the phase data, thereby indicating that the temperature changes are really not representative of what is actually occurring.

As long as large numbers of pixels are not dropping out, everything appears stable to the operator and/or the workstation through monitoring of the data, and the predefined minimum number of reference points remain available, the operator may provide instructions to proceed to the Stage 3 temperature display and treatment mode. However, if too many pixels have dropped out and/or the predefined minimum number of reference points is not available, then additional reference points should be selected prior to proceeding to Stage 3. The workstation can inhibit the operator from proceeding until further reference points are selected. Moreover, the workstation can select reference points or identify reference points for the operator, which the operator can confirm.

Once Stage 3 is entered, the operator may initially be required to enter the appropriate baseline temperature, such as 37° C., for the brain tissue in the illustrated example. Since all of the required reference points have been collected prior to proceeding to Stage 3, there is no need to select additional reference points. The selection can be locked by the workstation.

In Stage 3, the actual tissue temperature is now displayed instead of merely the mask. Thus, in the illustrated example, Stage 3 includes the computation of thermal damage. That is, a real temperature is actually being computed and retained in Stage 3, and is not used as a mask. In one exemplary implementation, the thermal damage or "dose" may be computed using an Arrhenius-type relationship between time and tissue temperature. This allows the operator to view temperature

maps of the brain tissue illustrating predictive damage that the software has calculated based on the sequencing of MRI data while providing the required treatment.

Also in Stage 3, a corrected phase is calculated as per Stage 2. A drift compensated phase difference is calculated by subtracting a baseline phase from the corrected phase. A current absolute temperature is calculated by adding a baseline temperature to a multiplication of the PRF factor and the drift compensated phase difference.

Thermal damage can be computed by a piecewise integration method. One method is to calculate an equivalent amount of time "t" (in minutes, hours or seconds) a tissue has been held at a specified temperature "T", which can be expressed as $t_{T,i}$. This specified temperature can represent a temperature above the baseline temperature, and/or a temperature at which thermal damage can be caused. Exemplary temperatures include 41° C., 42° C., 43° C., 44° C., 45° C., 46° C., 47° C., 48° C., 49° C., 50° C., 51° C., -60° C., 42° C.-46° C., or any fractional temperatures or ranges therebetween. "i" can refer to a time point or measurement number. A constant (R) is integrated according to the time point/measurement number and a difference between the specific temperature t and an actual temperature to compute thermal damage.

The constant R can be defined as a constant having values that are dependent on a current temperature, and thus, in some aspects can be a constant that varies according to a step function based on a current temperature. Tissue damage can be a complex function of time-temperature history, and the calculation of thermal damage can compare a time required for thermal injury to a reference temperature, based on findings that, for most soft tissue, a temperature above the specified temperature, such as 42° C., 43° C., 44° C., 45° C. or 46° C., causes thermal injury to the tissue.

A calculation of $t_{T,i}$ can be equated to one of various threshold times that can be indicated by one or more colored lines to indicate a tissue or portion of a tissue has been held at an equivalent temperature of the specified temperature for that threshold time. Adverting back to FIG. 100, the isoline or contour line 656 is displayed so as to coincide with a tissue or portions of a tissue that reach a first threshold.

Multiple isolines or contour lines can be simultaneously displayed in the GUI, where each of the lines corresponds to a different threshold. Exemplary thresholds can be set at 1, 2, 3, 4, 5, 10, 15, 20, 30, 45 and 60 minutes for specified temperatures of 42° C., 43° C., 44° C., 45° C. or 46° C. With such lines, such as two or three, being displayed simultaneously or contemporaneously, a progression of treatment can be monitored by an operator. Preferably one or more of the thresholds corresponds to a 100% or near 100% "kill rate" in that all or generally all biological functions of a tissue is destroyed at that amount of exposure to energy. However, other thresholds can be set to monitor treatment.

For cooling probes, an opposing relationship is viewable via the GUI for monitoring an equivalent temperature below the baseline temperature that indicates treatment or necrotizing of a tissue.

Through noise masking, real-time shaping is enabled to monitor treatment through a graphical user interface or other display. Color maps can be utilized in conjunction with isolines and/or contour lines that indicate a treatment shape. By tracking a probe position within tissue through feedback, multiple data slices provided around the probe position can be processed to monitor treatment and view thermal data. Thus, noise masking in combination with real-time probe feedback enables the calculation and display of real-time shaping of a treatment region. Further, real-time shaping utilizes multiple slices of image data and noise masking.

vii. Forecasting

Forecasting errors and issues with the MRI systems and various components is preferable to avoid procedure interruption. Forecasting can include continuous data filtration in connection with real-time shaping data rendering.

The workstation, either alone or in combination with a workstation or processing system dedicated to the MRI, monitors the reception of real time data from the MRI system. Based on statistics and averages of time delays (e.g., a latency) in receiving data (i.e., images) from the MRI system, a warning signal can be issued or displayed to an operator when a delay in receiving an expected image exceeds a threshold value. Based on a magnitude of the delay or repeating delays, the workstation can deactivate an energy output of a probe, and place the GUI of the workstation in a standby mode.

Similarly, the workstation can monitor temperature fluctuations in one or more of the reference points, within the patient, the MRI control room, the MRI system room or any other room. Excessive temperature fluctuations of tissue within the patient or within any of the rooms can indicate issues with the various components or accessory devices. Accordingly, based on a magnitude of the fluctuations of temperature in the reference points or any monitored area or portion of the patient, the workstation can deactivate an energy output of a probe, and place the GUI of the workstation in a standby mode.

A signal strength from the MRI is also monitored by the workstation. If a signal strength is too low, temperature data is unreliable and the operator is warned of the issue. Based on a magnitude of the signal strength, the workstation can deactivate an energy output of a probe, and place the (GUI of the workstation in a standby mode.

An image quality of the images received by the workstation can be monitored and measured for quality. Quality measuring identifies potentially harmful issues such as patient motion, RF noise, and other artifacts due to external causes. For example, a non-MRI compatible device or equipment near the patient can cause such artifacts. Quality measuring can include scanning received images to detect artifacts or unexpected pixel information. Based on image quality, the workstation can deactivate an energy output of a probe, and place the GUI of the workstation in a standby mode.

Once in standby mode, the workstation can automatically recover to resume treatment by selecting a new reference point and/or adjusting a noise mask, and then the operator can recommence treatment after confirming any data errors have been addressed and treatment of the patient is not impaired.

The workstation, either alone or in combination with a workstation or processing system dedicated to the MRI, can also perform signal filtration of MR raw data. The filtration can help identify issues that impact temperature sensitivity, accuracy and the ultimate prediction of thermal dose. Features or parts of a signal that are filtered include: range, outliers, sequence, and notification packets. These features or parts are processed by an algorithm of the workstation to collect, filter, sort and weight data. A corresponding display is displayed to an operator to inform the operator of potential issues, and allow the operator to continue with a treatment, pause a treatment or halt a treatment. The workstation can also provide recommendations for taking action based on predefined criteria and a history of analyzed data.

VII. Conclusion

The procedures and routines described herein can be embodied as a system, method or computer program product, and can be executed via one or more dedicated circuits or programmed processors. Accordingly, the descriptions pro-

vided herein may take the form of exclusively hardware, exclusively software executed on hardware (including firmware, resident software, micro-code, etc.), or through a combination of dedicated hardware components and general processors that are configured by specific algorithms and process codes. Hardware components are referred to as a "circuit," "module," "unit," "device," or "system." Executable code that is executed by hardware is embodied on a tangible memory device, such as a computer program product. Examples include CDs, DVDs, flash drives, hard disk units, ROMs, RAMs and other memory devices.

Reference has been made to flowchart illustrations and block diagrams of methods, systems and computer program products according to implementations of this disclosure. Aspects thereof are implemented by computer program instructions. These computer program instructions may be provided to a processor of a general purpose computer, special purpose computer, or other programmable data processing apparatus to produce a machine, such that the instructions, which execute via the processor of the computer or other programmable data processing apparatus, create means for implementing the functions/acts specified in the flowchart and/or block diagram block or blocks.

These computer program instructions may also be stored in a computer-readable medium that can direct a computer or other programmable data processing apparatus to function in a particular manner, such that the instructions stored in the computer-readable medium produce an article of manufacture including instruction means which implement the function/act specified in the flowchart and/or block diagram block or blocks.

The computer program instructions may also be loaded onto a computer or other programmable data processing apparatus to cause a series of operational steps to be performed on the computer or other programmable apparatus to produce a computer implemented process such that the instructions which execute on the computer or other programmable apparatus provide processes for implementing the functions/acts specified in the flowchart and/or block diagram block or blocks.

A number of implementations have been described. Nevertheless, it will be understood that various modifications may be made without departing from the spirit and scope of this disclosure. For example, preferable results may be achieved if the steps of the disclosed techniques were performed in a different sequence, if components in the disclosed systems were combined in a different manner, or if the components were replaced or supplemented by other components. The functions, processes and algorithms described herein may be performed in hardware or software executed by hardware, including computer processors and/or programmable circuits configured to execute program code and/or computer instructions to execute the functions, processes and algorithms described herein. Additionally, some implementations may be performed on modules or hardware not identical to those described. Accordingly, other implementations are within the scope that may be claimed.

A system for effecting treatment to a tissue can include: an automated drive mechanism including a holder to hold a treatment device, wherein the drive mechanism is coupled to one or more wires such that a translation of the one or more wires effects one or more of a longitudinal displacement of the holder and a rotation of the holder; and a controller including an input interface to process position control signals for setting a position of the treatment device, and an output interface to translate the one or more wires based on the position control signals.

The system can further include: a guide mechanism that is attachable to a surface of a patient, wherein the guide mechanism includes a base structure that is configured to remain stationary relative to the patient when the guide mechanism is attached to the surface of the patient in a locked state, the guide mechanism includes a tilt portion that is coupled to the base structure, the tilt portion is structured so as to hold the drive mechanism at a position that is separated from the surface of the patient, and the tilt portion provides an adjustable tilt between a trajectory of the drive mechanism and the base structure. The guide mechanism can further include a rotation portion that provides an adjustable rotation of the tilt portion relative to the base structure.

The drive mechanism can be motorless and consists of thermal imaging compatible components.

The controller can be configured to process a sequence of the position control signals to: move the holder to a first position for effecting the treatment to the tissue at a first portion of the tissue that coincides with the first position; and move the holder to a second position for effecting the treatment to the tissue at a second portion of the tissue that coincides with the second position. The system can further include a workstation to transmit the position control signals to the controller and to display thermometry images of the tissue. The workstation can continuously display the thermometry images of the tissue during the treatment to the tissue at the first and second portions of the tissue, and while the holder moves between the first and second positions.

The system can further include an energy emission probe as the treatment device, wherein the probe generates a plurality of different output patterns. The probe can include a first laser fiber for outputting a symmetrical output pattern with respect to a longitudinal axis of the first laser fiber, and the probe can include a second laser fiber for outputting an asymmetrical output pattern with respect to a longitudinal axis of the second laser fiber.

The system can further include: an energy source to generate energy for the probe; and a workstation to transmit the position control signals to the controller, and to transmit energy control signals to the energy source, wherein the workstation is configured to process a sequence of the energy control signals to: effect a symmetrical treatment to the tissue with the probe; and effect an asymmetrical treatment to the tissue with the probe after the symmetrical treatment.

The system can also include: a laser source to generate laser energy for the laser probe; and a workstation to transmit the position control signals to the controller, and to transmit laser control signals to the laser source, wherein the workstation is configured to process a sequence of the position and laser control signals to: move the holder to a first position for effecting the treatment to the tissue at a first portion of the tissue that coincides with the first position; effect a symmetrical treatment to the first portion of the tissue with the first laser fiber; move the holder to a second position for effecting the treatment to the tissue at a second portion of the tissue that coincides with the second position; and effect an asymmetrical treatment to the second portion of the tissue with the second laser fiber. The workstation can be configured to display thermometry images of the tissue continuously throughout processing of the sequence of the position and laser control signals and throughout moving the holder and effecting the symmetrical and asymmetrical treatments.

The system can include an imaging system to output images of the tissue and the treatment device, including thermometry images of the tissue, in real time, continuously throughout one or more steps of effecting the treatment to the tissue; and a workstation to transmit the position control

signals to the controller based on one or more of the images, as the images are received by the workstation in real time, and to display, in real time, one or more of the images throughout the one or more steps of effecting the treatment to the tissue.

The workstation can be configured to display, in real time, the thermometry images of the tissue with the images of the tissue and the treatment device continuously throughout a processing of the position control signals and throughout moving the holder and effecting the treatment to the tissue.

The workstation can be configured to process, in real time, the images of the tissue and the treatment device and the thermometry images of the tissue to forecast errors or interruptions in the treatment to the tissue and display a corresponding warning.

The system can further include an energy emission probe as the treatment device, the energy emission probe including one or more emitters selected from: a laser fiber, a radiofrequency emitter, a high-intensity focused ultrasound emitter, a microwave emitter, a cryogenic cooling device, and a photodynamic therapy light emitter. The energy emission probe can include a plurality of the emitters. The plurality of the emitters can be longitudinally spaced with respect to a longitudinal axis of the energy emission probe.

The system can further include a guide sheath including a plurality of probes of different modalities as the treatment device, wherein the modalities include one or more of: laser, radiofrequency, high-intensity focused ultrasound, microwave, cryogenic, photodynamic therapy, chemical release and drug release. The guide sheath can include one or more off-axis holes for positioning an emitting point of one or more of the plurality of probes at an off-axis angle.

The invention claimed is:

1. A method for thermal monitoring of tissue during thermal therapy, comprising:

prior to initiation of thermal therapy,

obtaining, by processing circuitry, a plurality of magnetic resonance (MR) images of a patient, wherein the plurality of MR images correspond to a same imaging slice captured over a time period, and each MR image of the plurality of MR images includes respective phase data,

identifying, by the processing circuitry, a volume in the patient corresponding to a) a region of interest at which to apply thermal therapy and b) surrounding tissue,

analyzing, by the processing circuitry, pixel locations of the phase data of the plurality of MR images corresponding to the volume to identify one or more pixel locations demonstrating excessive phase noise,

determining, by the processing circuitry, a noise mask for the region of interest, wherein the noise mask excludes the one or more pixel locations demonstrating excessive phase noise, and

selecting, from the pixels included in the noise mask, a plurality of reference points, wherein the plurality of reference points identify locations within the surrounding tissue, and

each reference point of the plurality of reference points corresponds to a particular pixel location of the phase data having a particular phase value; and

initiating monitoring of the thermal therapy, wherein monitoring comprises

receiving a current MR image of the patient,

adjusting, by the processing circuitry, the phase data of the current MR image according to the plurality of reference points, wherein adjusting the phase data of the current MR image comprises

determining, based upon at least a subset of the plurality of reference points without considering phase data corresponding to pixel locations within the region of interest, a plurality of phase drift values to correct for phase drift, and
 5 extrapolating the phase drift values into a phase map, wherein at least a portion of the phase map corresponds to the pixel locations within the region of interest,
 10 applying, by the processing circuitry, the phase map to the current phase data to obtain drift-adjusted phase data, and
 15 calculating, by the processing circuitry, a temperature map using the drift-adjusted phase data, wherein the temperature map corresponds to at least the region of interest.

2. The method of claim 1, further comprising, after determining the noise mask and prior to initiating thermal therapy, displaying, on a graphical user interface, a rendering of the noise mask overlaying the volume in the patient in a first MR image of the plurality of MR images.

3. The method of claim 2, wherein selecting the plurality of reference points comprises receiving, via interaction with the graphical user interface, a respective user selection of each of the plurality of reference points from the rendering of the noise mask.

4. The method of claim 1, wherein selecting the plurality of reference points comprises automatically selecting, by the processing circuitry independently of user selection, at least a portion of the plurality of reference points.

5. The method of claim 4, further comprising receiving user input confirming acceptance of the automatically selected reference points of the plurality of reference points.

6. The method of claim 1, wherein selecting the plurality of reference points comprises verifying, by the processing circuitry, that each reference point of the plurality of reference points corresponds to a respective tissue region of a same tissue type as the remaining reference points.

7. The method of claim 1, wherein the plurality of MR images comprises at least three MR images.

8. The method of claim 1, further comprising, prior to initiation of thermal therapy:
 validating, by the processing circuitry, stability of drift-adjusted phase data, wherein
 45 validating the stability of drift-adjusted phase data comprises
 obtaining a present MRI image of the volume;
 computing, at every location within the volume, a respective temperature difference from a reference tissue temperature, wherein computing the respective temperature difference comprises adjusting the phase data of the present MR image according to the plurality of reference points;
 50 applying, to the respective temperature differences, a temperature variance threshold to identify a plurality of noisy locations; and
 illustrating, on a graphical user interface, a rendering of a temperature mask overlaying the volume in the patient, wherein the noisy locations are specified by visual indications.

9. The method of claim 8, wherein the noisy locations are indicated by transparent portions of a color overlay.

10. A system for thermal monitoring of tissue during thermal therapy, comprising:
 65 a processor in communication with a display and a magnetic resonance (MR) imaging device; and

a memory having instructions stored thereon, wherein the instructions, when executed by the processor, cause the processor to:
 prior to initiation of thermal therapy,
 5 obtain, from the MR imaging device, a plurality of magnetic resonance (MR) images of a patient, wherein
 the plurality of MR images correspond to a same imaging slice over a time period, and
 10 each MR image of the plurality of MR images includes respective magnetic resonance (MR) phase data,
 15 identify a volume in the patient corresponding to a) a region of interest at which to apply thermal therapy and b) surrounding tissue, wherein the plurality of MR images comprises respective magnetic resonance (MR) image data representing a portion of the volume including a portion of the region of interest, and
 determine a plurality of reference points, wherein
 the plurality of reference points identify locations within the surrounding tissue, and
 each reference point of the plurality of reference points corresponds to a particular pixel location of the phase data having a particular phase value; and
 initiate monitoring of thermal therapy, wherein monitoring comprises
 receiving, from the MR imaging device, a current MR image of the patient,
 calculating a plurality of phase drift values associated with the plurality of reference points, wherein the phase drift values are based upon phase values of each respective reference point of the plurality of reference points over successive magnetic resonance (MR) phase data of the current MR image and a former MR image without considering phase data corresponding to pixel locations within the region of interest,
 extrapolating the phase drift values of the plurality of reference points into a phase map, wherein at least a portion of the phase map corresponds to the pixel locations within the region of interest,
 applying the phase map to the MR phase data of the current MR image to obtain drift-compensated phase data,
 calculating a temperature map based upon the drift-compensated phase data, wherein the temperature map corresponds to at least the region of interest, and
 presenting, on the display, a rendering of the MR image including a graphical representation of temperatures in the region of interest according to the temperature map.

11. The system of claim 10, wherein the graphical representation of temperatures comprises a color overlay.

12. The system of claim 10, further comprising, prior to determining the plurality of reference points:
 analyzing the respective MR phase data of each MR image of the plurality of MR images to identify a plurality of noisy data points; and
 marking the plurality of noisy data points as ineligible for selection as reference points.

13. The system of claim 12, wherein identifying a particular noisy data point of the plurality of noisy data points comprises determining whether a difference of phase values of the

55

particular noisy data point between two MR images of the plurality of MR images exceeds a threshold level.

14. The system of claim 10, wherein calculating the temperature map comprises multiplying the drift-compensated phase data by a constant and adding a baseline temperature of the volume.

15. The system of claim 14, wherein the instructions, when executed by the processor, cause the processor to receive, through a user interface, the baseline temperature.

16. The method of claim 8, further comprising; receiving, through a user interface responsive to illustrating the rendering of the temperature mask, user input modifying the plurality of reference points, wherein the user input corresponds to at least one of a) a deletion of a first reference point of the plurality of reference points, and b) an addition of a new reference point to the plurality of reference points; and

56

repeating validation of stability of the drift-adjusted phase data using the modified plurality of reference points.

17. The method of claim 8, further comprising receiving, through a user interface prior to validating the stability of the drift-adjusted phase data, the reference tissue temperature.

18. The system of claim 10, wherein the plurality of reference points comprises fewer than twenty-five reference points.

19. The system of claim 10, wherein:

the plurality of reference points comprises at least eight reference points; and
extrapolating the phase drift values into the phase map comprises applying the phase drift values to the phase data using a polynomial surface fit.

20. The method of claim 6, wherein the tissue type is brain tissue.

* * * * *

专利名称(译)	监测和隔热治疗热疗		
公开(公告)号	US9271794	公开(公告)日	2016-03-01
申请号	US14/557127	申请日	2014-12-01
[标]申请(专利权)人(译)	曼特瑞斯醫藥有限責任公司		
申请(专利权)人(译)	MONTERIS医疗法人		
当前申请(专利权)人(译)	MONTERIS医疗法人		
[标]发明人	TYC RICHARD QURESHI SALMAN GRANT MARK ANDREW FERNANDES LUIS FILIPE SILVA CARREIRA DANIEL PRAZERES SCHELLHORN JOHN		
发明人	TYC, RICHARD QURESHI, SALMAN GRANT, MARK, ANDREW FERNANDES, LUIS, FILIPE, SILVA CARREIRA, DANIEL, PRAZERES SCHELLHORN, JOHN		
IPC分类号	A61B18/00 A61N5/06 A61N7/02 A61B18/28 A61B18/18 A61B18/14 A61B18/06 A61B18/02 A61B18/20 A61B18/22 A61B5/01 A61B17/00 G01R33/48 G01R33/28 A61B5/00 A61B17/3207 A61B17/34 A61B5/055		
CPC分类号	A61B18/22 A61B5/015 A61B5/055 A61B5/4839 A61B5/742 A61B5/746 A61B18/02 A61B18/0206 A61B18/06 A61B18/148 A61B18/1492 A61B18/1815 A61B18/20 A61B18/28 A61B34/71 A61B90/10 A61N5/0601 A61N5/062 A61N7/022 G01R33/285 G01R33/4804 A61B2017/00017 A61B2017/3407 A61B2018/00017 A61B2018/00023 A61B2018/00446 A61B2018/00577 A61B2018/00642 A61B2018/00791 A61B2018/00994 A61B2018/0212 A61B2018/0293 A61B2018/1807 A61B2018/1861 A61B2018/2085 A61B2018/2211 A61B2018/2261 A61B19/201 A61B19/20 A61B19/56 A61B2019/5268 A61B19/203 A61B2019/2211 A61B2019/5236 A61B19/5244 A61B2019/461 A61B2034/2068 A61B2017/00911 A61B34/25 A61B90/11 A61B90/14 A61B2018/20351 A61B2034/107 A61B2034/301 A61B2090/374 A61B34/20 A61B2090/061 A61B2018/00702		
优先权	61/759197 2013-01-31 US 61/728068 2012-11-19 US 61/664791 2012-06-27 US		
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外部链接	Espacenet USPTO		

摘要(译)

组织的图像引导治疗可以利用磁共振成像 (MRI) 或其他医学成像设备来引导组织内的器械。工作站可以致动器械的运动，并且可以致动器械的能量发射和/或冷却以实现组织的治疗。该仪器可以是MRI兼容的激光探针，其例如为患者脑中的组织提供热疗。通过反馈跟踪组织内的探针位置，可以处理在探针位置周围提供的多个数据切片以监测治疗和查看热数据。操作者在噪声掩蔽的帮助下选择治疗区域参考点。

