



US 20150305671A1

(19) **United States**
(12) **Patent Application Publication**
Yoon et al.

(10) **Pub. No.: US 2015/0305671 A1**
(43) **Pub. Date: Oct. 29, 2015**

(54) **SMART DIAGNOSTIC MOUTH GUARD SYSTEM**

A61M 21/02 (2006.01)
A61F 5/56 (2006.01)

(71) Applicant: **UNIVERSITY OF FLORIDA RESEARCH FOUNDATION, INC.**,
Gainesville, FL (US)

(52) **U.S. Cl.**
CPC *A61B 5/4557* (2013.01); *A61F 5/566* (2013.01); *A61B 5/682* (2013.01); *A61B 5/01* (2013.01); *A61B 5/0008* (2013.01); *A61B 5/486* (2013.01); *A61B 5/7455* (2013.01); *A61B 5/7282* (2013.01); *A61M 21/02* (2013.01); *A61B 5/742* (2013.01); *A61B 5/7475* (2013.01); *A61B 5/681* (2013.01); *A61B 5/6898* (2013.01); *A61B 5/4836* (2013.01); *A61F 2005/563* (2013.01); *A61B 2562/0219* (2013.01); *A61M 2021/0027* (2013.01)

(72) Inventors: **Yong-Kyu Yoon**, Gainesville, FL (US);
Xiaoyu Cheng, Gainesville, FL (US);
Gloria Jung-a Kim, Gainesville, FL (US);
Fong Wong, Ocala, FL (US)

(21) Appl. No.: **14/760,641**

(22) PCT Filed: **Jan. 14, 2014**

(86) PCT No.: **PCT/US2014/011409**

§ 371 (c)(1),
(2) Date: **Jul. 13, 2015**

Related U.S. Application Data

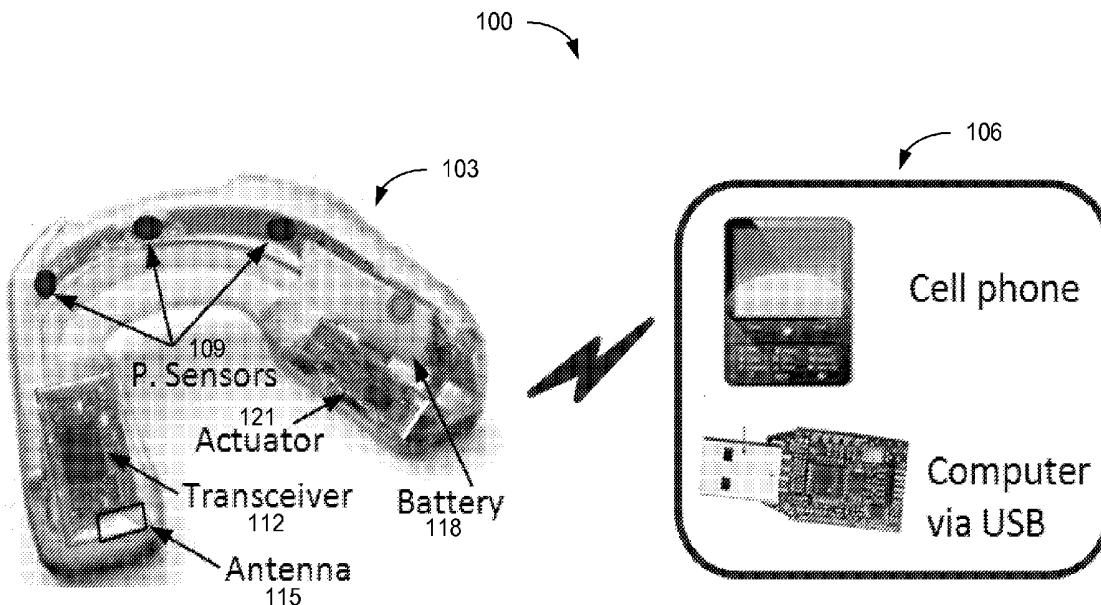
(60) Provisional application No. 61/752,142, filed on Jan. 14, 2013.

Publication Classification

(51) **Int. Cl.**
A61B 5/00 (2006.01)
A61B 5/01 (2006.01)

(57) **ABSTRACT**

Various examples are provided for a smart mouth guard for diagnosis, quantification, and/or management of e.g., bruxism. In one example, among others, a diagnostic mouth guard includes a plurality of pressure sensors and processing circuitry configured to provide pressure sensor data to an external processing unit when located in an oral cavity. The diagnostic mouth guard may also include temperature, pH and/or inertia sensors. In another example, a system includes the diagnostic mouth guard and the external processing unit such as, e.g., a smart phone, table or computer. The diagnostic mouth guard can communicate with the external processing unit over a wireless channel.



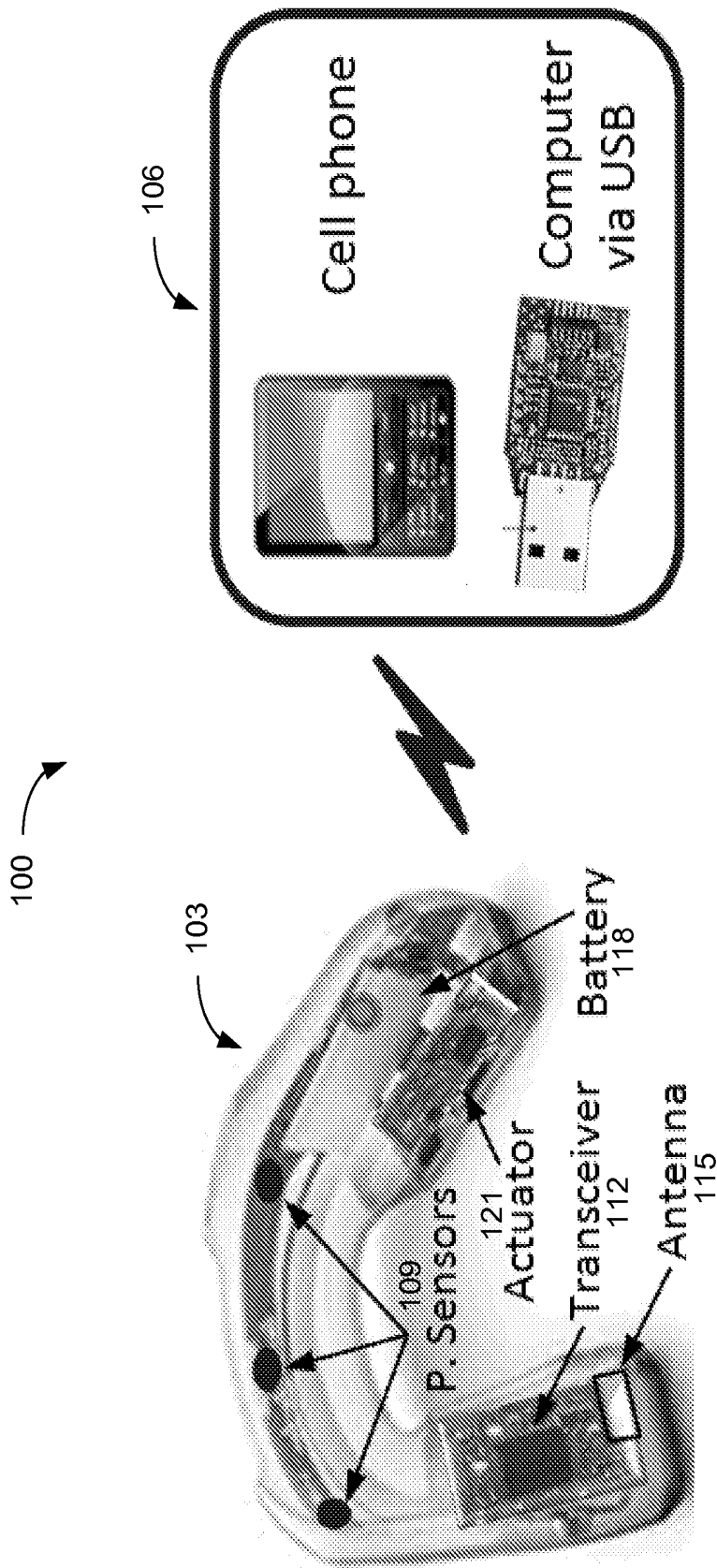


FIG. 1

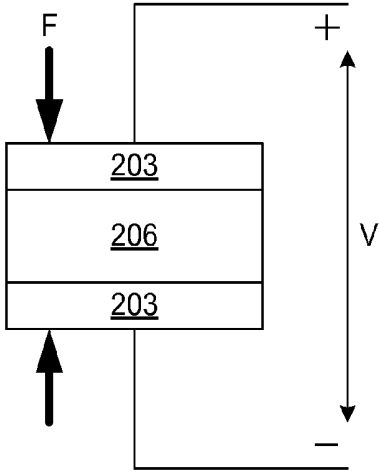


FIG. 2A

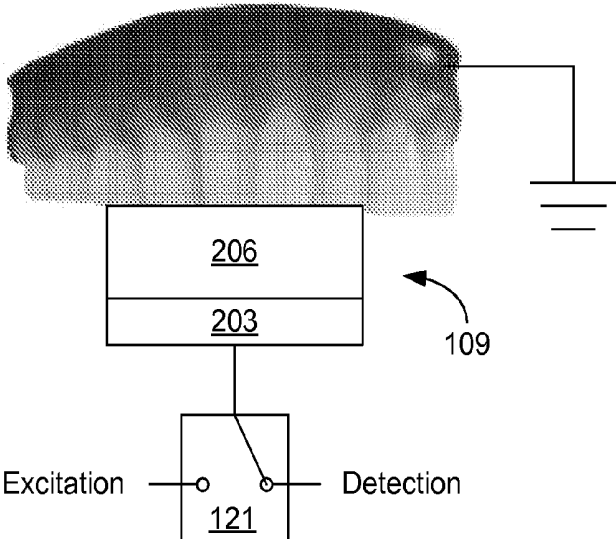


FIG. 2B

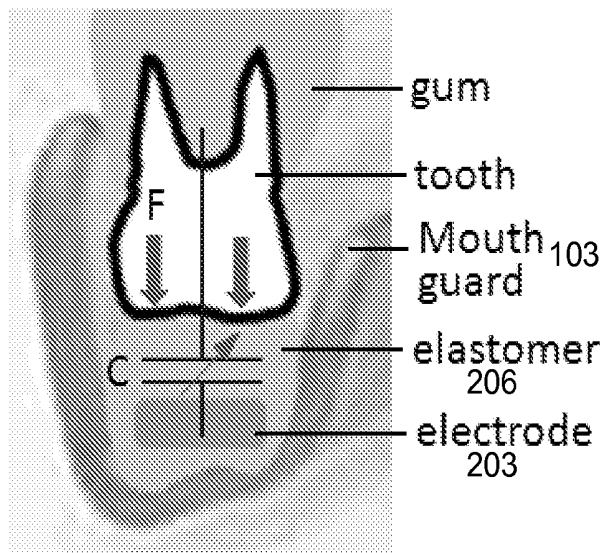


FIG. 3

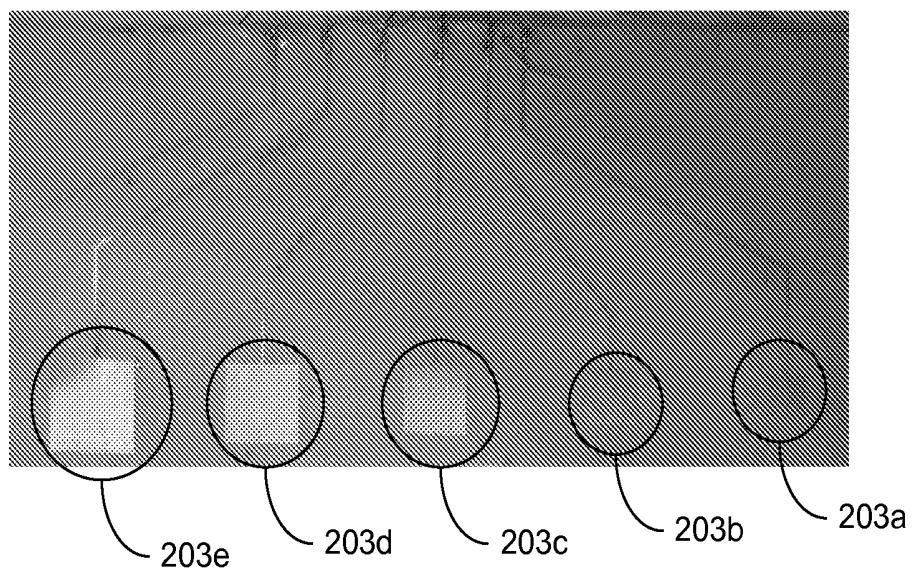


FIG. 4A



FIG. 4B

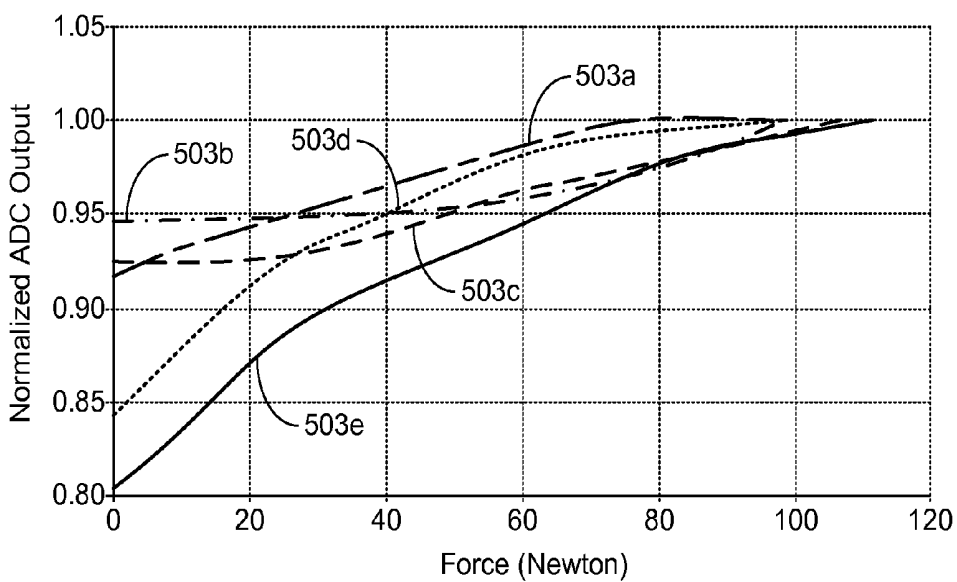


FIG. 5A

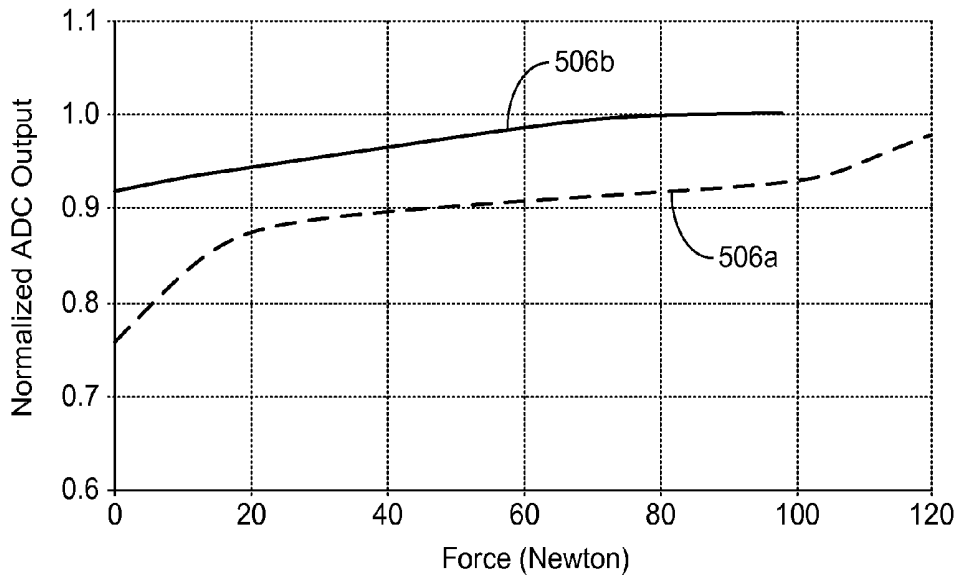


FIG. 5B

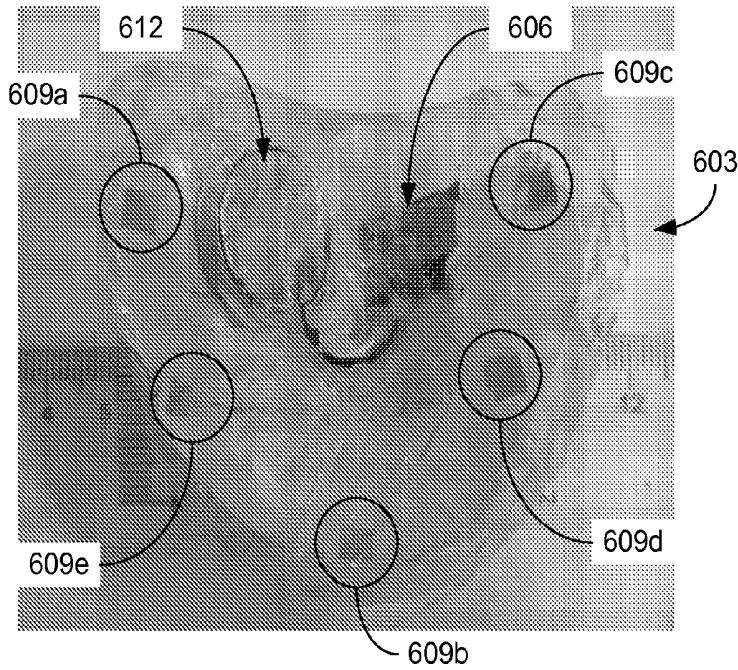


FIG. 6A

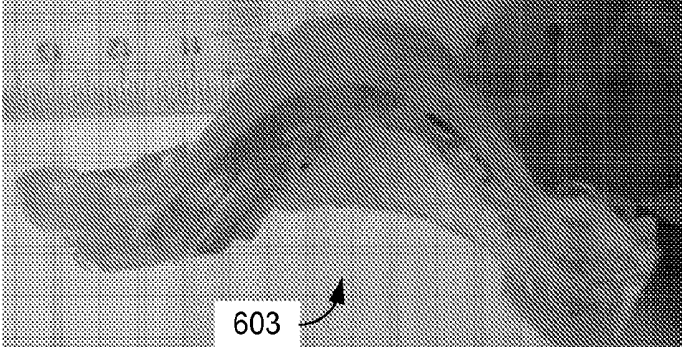


FIG. 6B

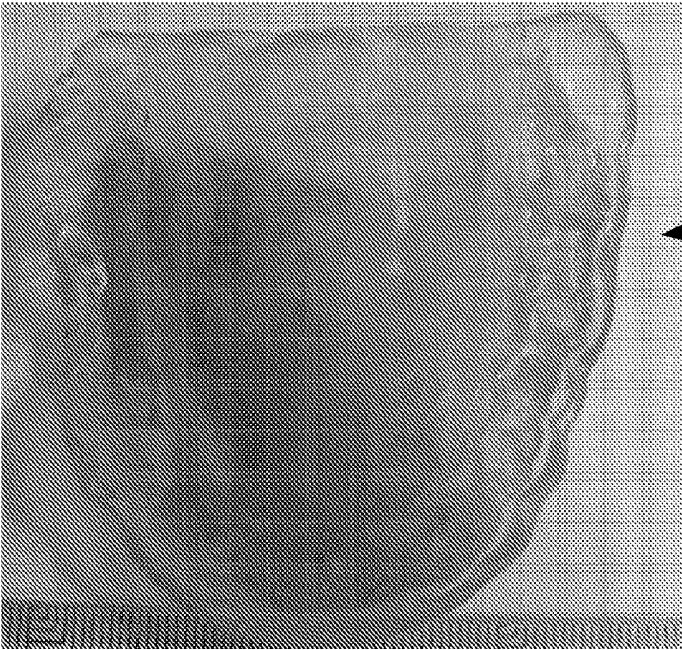


FIG. 6C

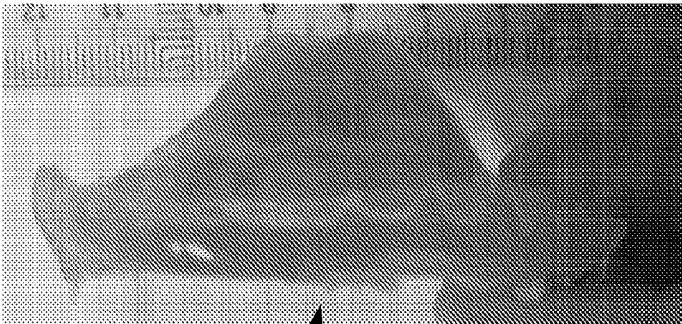


FIG. 6D

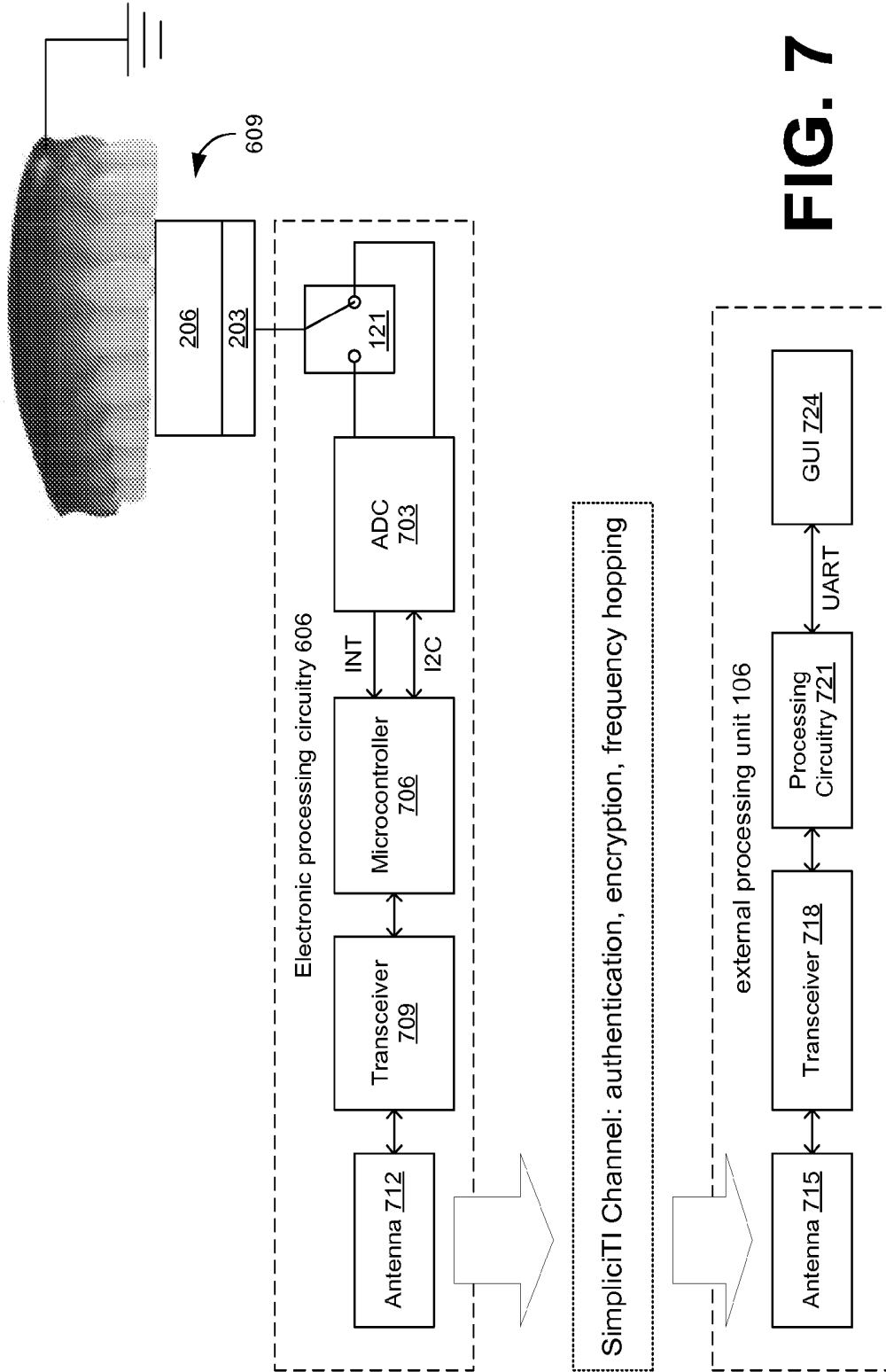


FIG. 7

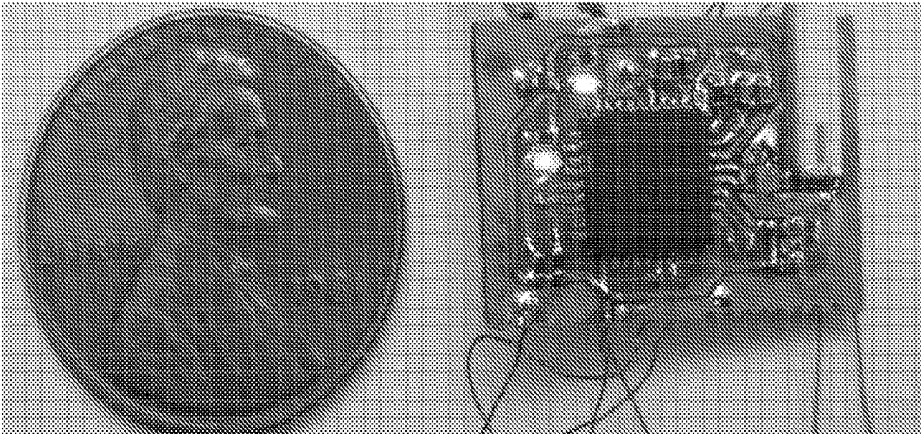


FIG. 8A

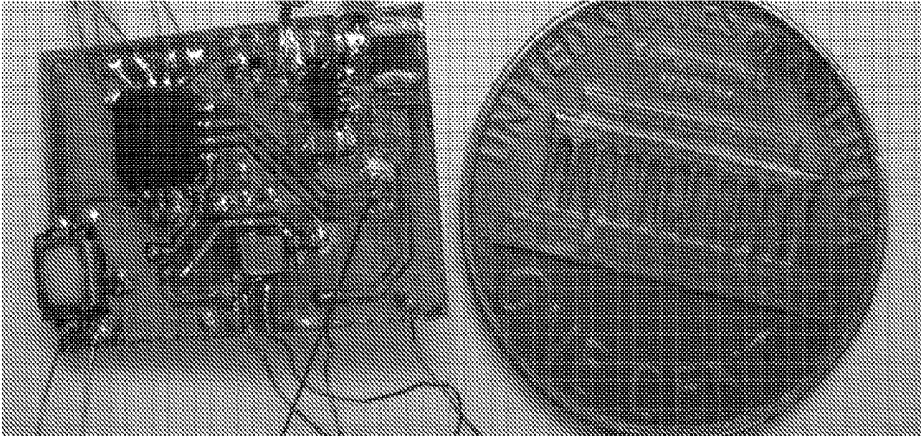


FIG. 8B

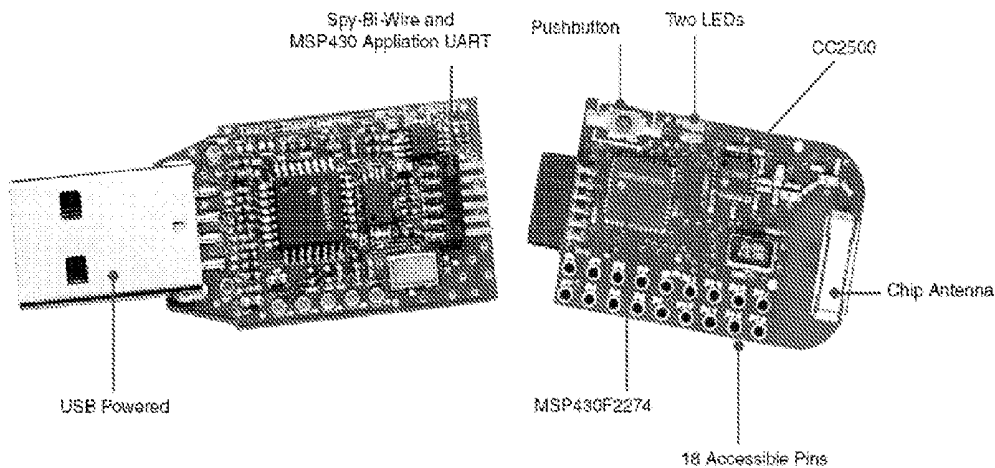


FIG. 9

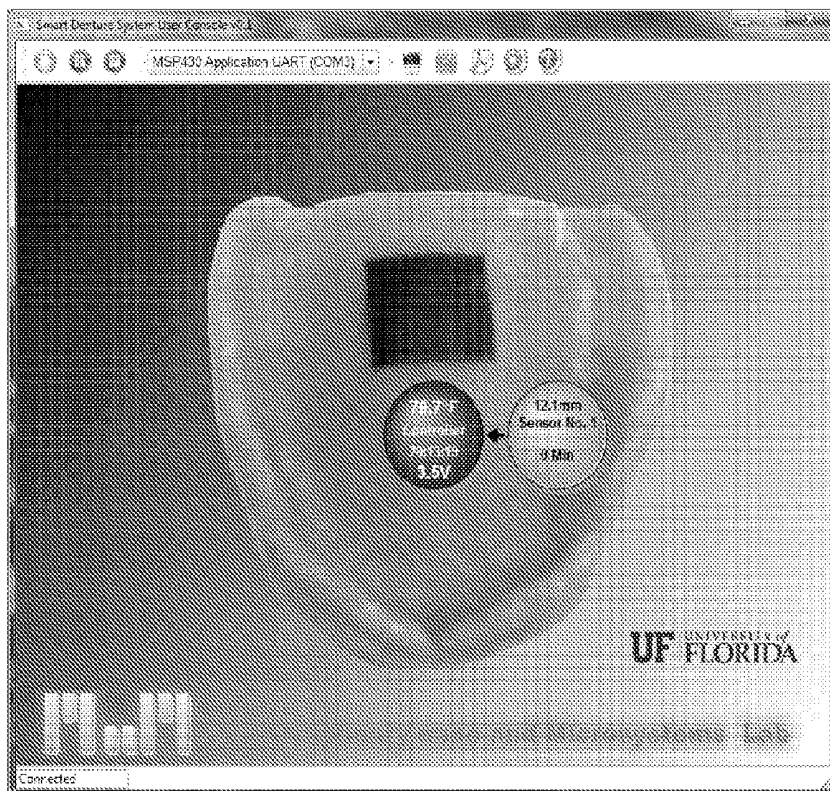


FIG. 10

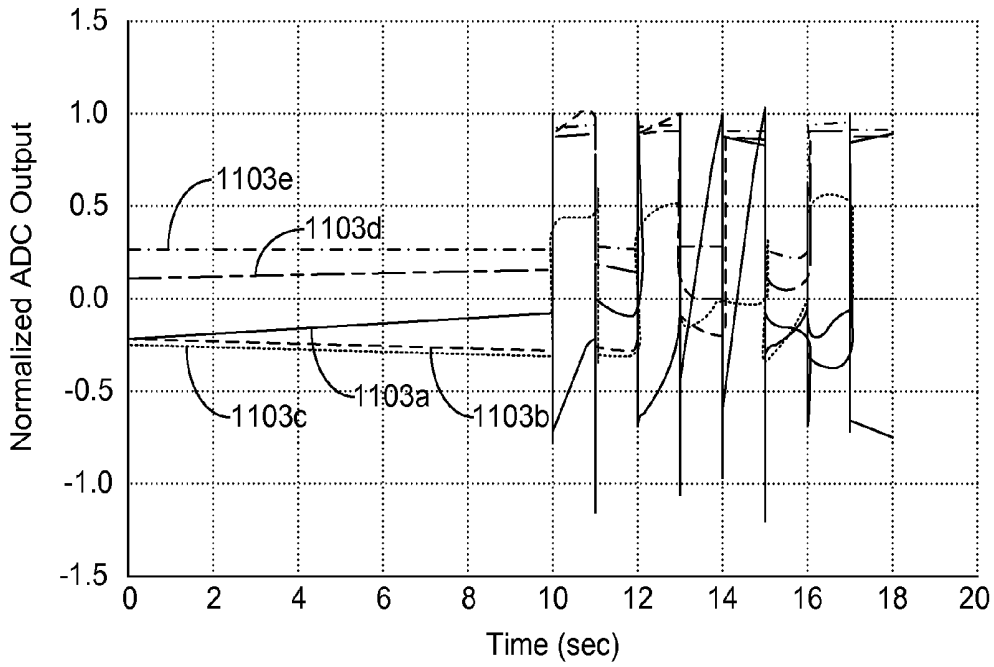


FIG. 11A

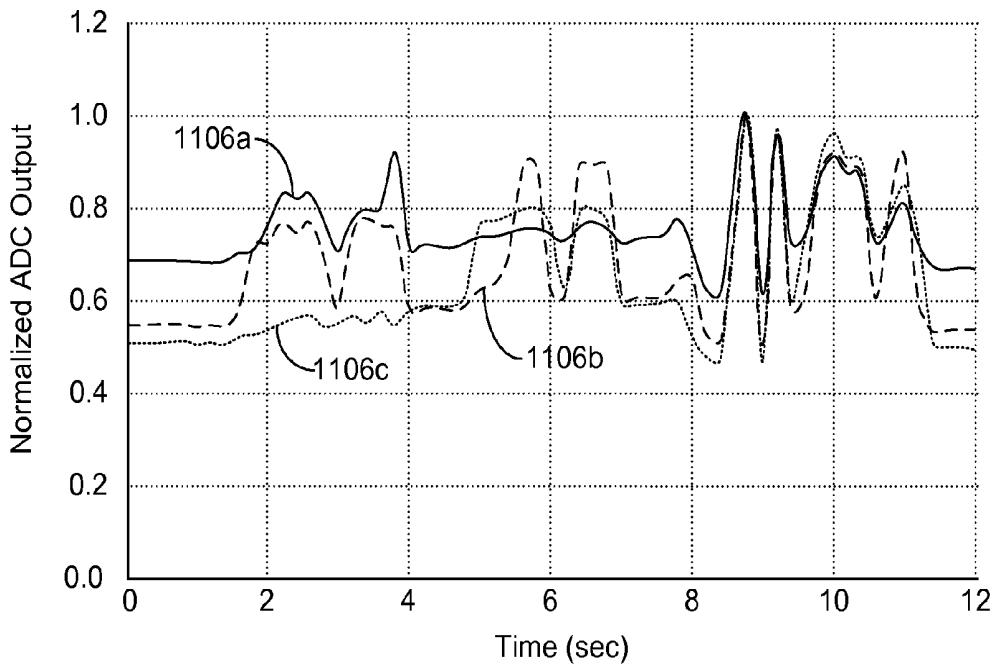


FIG. 11B

SMART DIAGNOSTIC MOUTH GUARD SYSTEM

CROSS REFERENCE TO RELATED APPLICATIONS

[0001] This application claims priority to and the benefit of co-pending U.S. provisional application entitled “SMART DIAGNOSTIC MOUTH GUARD SYSTEM” having Ser. No. 61/752,142, filed Jan. 14, 2013, which is hereby incorporated by reference in its entirety.

BACKGROUND

[0002] Chronic stress is a major cause of chronic illness, which in turn is a major driver of escalating health care costs in the US. Many Americans are living with moderate or high levels of stress. Since assessment of chronic stress depends almost exclusively on retrospective self-reporting, under-reporting poses a serious impediment to clinical assessment, early intervention, and primary prevention. Among the many symptoms and pathological consequences of stress, nocturnal bruxism has drawn attention from many clinicians in related fields.

[0003] Bruxism is characterized by the grinding of the teeth and typically includes the clenching of the jaw. Bruxism normally occurs during sleep and can result in a variety of health issues. The etiology of bruxism is unclear and varied, but it has been known to manifest in tooth wear, signs and symptoms of temporomandibular disorders (TMD), headaches, toothache, mobile teeth, and various problems with dental restorations as well as with fixed and removable prostheses. Dentists have relied on polysomnography and various versions of electromyography (EMG) to ascertain, diagnose, approximate the extent of, and reduce nocturnal bruxism.

BRIEF DESCRIPTION OF THE DRAWINGS

[0004] Many aspects of the present disclosure can be better understood with reference to the following drawings. The components in the drawings are not necessarily to scale, emphasis instead being placed upon clearly illustrating the principles of the present disclosure. Moreover, in the drawings, like reference numerals designate corresponding parts throughout the several views.

[0005] FIG. 1 is an example of a smart mouth guard system (SMS) in accordance with various embodiments of the present disclosure.

[0006] FIGS. 2A and 2B are examples of capacitive pressure sensors in accordance with various embodiments of the present disclosure.

[0007] FIG. 3 is a graphical representation of a cross-sectional view illustrating capacitive pressure sensing by the mouth guard of the SMS of FIG. 1 in accordance with various embodiments of the present disclosure.

[0008] FIGS. 4A and 4B show example of conductive pads on a flexible substrate that may be used for capacitive pressure sensors in the SMS of FIG. 1 in accordance with various embodiments of the present disclosure.

[0009] FIGS. 5A and 5B are plots illustrating the effect of pad size and elastic material thickness on the capacitive pressure sensors of FIG. 1 in accordance with various embodiments of the present disclosure.

[0010] FIGS. 6A-6D are images of an example of a mouth guard of the SMS of FIG. 1 in accordance with various embodiments of the present disclosure.

[0011] FIG. 7 is a graphical representation of an example of the SMS of FIG. 1 in accordance with various embodiments of the present disclosure.

[0012] FIGS. 8A and 8B are images of an example of electronic processing circuitry of the SMS mouth guard of FIG. 7 in accordance with various embodiments of the present disclosure.

[0013] FIG. 9 is an example of a transceiver and antenna used in an external processing unit of the SMS of FIG. 1 in accordance with various embodiments of the present disclosure.

[0014] FIG. 10 is an example of a graphical user interface shown on a display (e.g., a computer screen or smart phone display) of the SMS of FIG. 1 in accordance with various embodiments of the present disclosure.

[0015] FIGS. 11A and 11B are plots of examples of pressure sensor data obtained by the SMS of FIG. 1 in accordance with various embodiments of the present disclosure.

DETAILED DESCRIPTION

[0016] Disclosed herein are various embodiments of related to a smart mouth guard for diagnosis, quantification, and/or management of, e.g., bruxism. Reference will now be made in detail to the description of the embodiments as illustrated in the drawings, wherein like reference numbers indicate like parts throughout the several views.

[0017] People bite, grind or clench their teeth for non-functional purposes throughout a day. This can happen to people of nearly all ages with an exerted biting force that can range from about 10 lbs. to about 200 lbs. Bruxism includes the activities of grinding or clenching the teeth and may result in excessive wear of the jaw joints, muscles and teeth, headache, depression, muscle soreness, and/or temporomandibular disorder.

[0018] A smart mouth guard system (SMS) capable of diagnosis, quantification, and management may be used in the identification and control of bruxism. The SMS provides the ability to measure human biting and clenching force in real-time and wirelessly transmit data from the mouth guard to an external processing unit such as, e.g., a personal computer, tablet, smart phone, smart watch, etc. Referring to FIG. 1, shown is an example of a SMS 100 including a mouth guard 103 (e.g., an occlusal splint) and an external processing unit 106 such as, e.g., a cell phone or a computer. The mouth guard 103 may include an array of capacitive pressure sensors 109, a wireless transceiver 112, an antenna 115, and a wireless power delivery/management system for the battery 118. In addition, the system may be equipped to monitor conditions of the oral environment, such as pH and temperature using appropriate sensors. Inertia sensors such as, e.g., accelerometers and/or gyroscopes may also be included in the mouth guard 103 to monitor motion and/or orientation of the wearer. An actuator 121 may be included that controls charging of and data acquisition from the pressure sensors 109 and/or other sensors of the mouth guard 103. The SMS 100 can utilize wireless telemetry such as, e.g., Bluetooth or near-field communication capabilities to communicate with the external processing unit 106 and/or a USB transceiver dongle which can be connected to, e.g., a personal computer or tablet. Applications (apps) or other programs executed by the external processing unit 106 can control communications between the mouth guard 103 and external processing unit 106 and/or data management. The SMS can simplify self-monitoring, provide customized feedback, and intervene—either auto-

matically prompt a clinician to intervene in person or through the apps executing on the external processing unit 106.

[0019] The capacitive pressure sensors 109 utilize capacitive based transducers that are incorporated into the mouth guard 103. Capacitive based transducers can provide good tactile or distance, strain, humidity, gas, pressure, and/or biomedical sensing. FIG. 2A illustrates an example of a floating sensor including two conductive pads 203 separated by an elastic material (or elastomer) 206. Force (F) applied to one or both of the conductive pads 203 compresses the elastic material 206 and changes the capacitance of the sensor 109. Knowing the characteristics of the elastic material 206 allows the capacitance of the pressure sensor 109 to be correlated to the applied force (F). The capacitance of the sensor 109 may be detected based on the voltage (V) between the conductive pads 203. A grounded sensor including a single conductive pad 203 may be used in a similar fashion.

[0020] Capacitance may be defined as:

$$C \triangleq \frac{q}{V}$$

and the two-dimensional (2D) surface charge density on a metal pad surface may be given by:

$$\rho_s = \frac{q}{A}$$

From Gauss's Law, the charge is given by:

$$q = \oint_S D \cdot dA$$

Using Maxwell's equation:

$$D = \epsilon E$$

we have:

$$E = \frac{q}{4\pi\epsilon r^2},$$

where ϵ is the permittivity. By substituting ρ_s into the equation, we obtain:

$$E = \frac{\rho_s A}{4\pi\epsilon r^2} = \frac{\rho_s}{\epsilon} = \frac{q}{\epsilon A}$$

[0021] Since:

$$V = -\int_0^t E \, dt = Et$$

then:

$$V = Et = \frac{qt}{\epsilon A} \text{ and } C = \frac{q}{V} = \frac{\epsilon A}{t}$$

which is identical to the floating configuration.

[0022] FIG. 2B illustrates an example of a grounded sensor including a single conductive pad 203. In the example of FIG. 2B, the second conductive plate is provided by the mouth of a user wearing the mouth guard 103, which is grounded. The elastic material 206 is biocompatible for use by the user.

When the user bites down on the elastic material 206, the capacitance of the pressure sensor varies with the applied pressure. Actuator 121 allows for charging of the conductive pad 203, followed by detection of the plate voltage variation.

[0023] Referring to FIG. 3, shown is a graphical representation of a cross-sectional view illustrating capacitive pressure sensing by the mouth guard 103 in accordance with various embodiments of the present disclosure. Included in the mouth guard 103 is a grounded sensor including a single conductive pad (or electrode) 203. The oral tissue (gum) and tooth serve as a counter electrode and an elastic polymeric material 206 (or elastomer such as, e.g., polydimethylsiloxane (PDMS), polymethylmethacrylate (PMMA), or a combination thereof) serves as a dielectric layer for the capacitor. Typical chewing pressure is in the range of about 10 lbs to about 200 lbs (about 100 kPa to about 2000 kPa). In order to address the bruxing pressure level, both silicone (polydimethylsiloxane: PDMS) with a thickness in the range of about 100 μ m to about 500 μ m and acrylic (polymethylmethacrylate: PMMA) with a thickness of about 100 μ m to about 500 μ m may be used, where the Young's modulus of PDMS and PMMA is 360 kPa and about 1800 kPa to about 3100 kPa, respectively. Both materials are biocompatible and are routinely used in restorative dentistry.

[0024] When a user bites down and/or grinds teeth (e.g., when bruxing occurs), the tooth exerts pressure on the elastomer material 206 underneath the tooth, changing the gap between the tooth and the electrode or conductive pad 203, resulting in a capacitance change. The capacitance change is proportional to the applied pressure and thus the bruxing level. By monitoring the capacitance change, it is possible to quantify the extent and severity of bruxism.

[0025] Capacitive pressure sensors 109 may be fabricated using a flexible printed circuit board including a flexible substrate (e.g., R03003 by Rogers Inc.). FIG. 4A shows an image of the conductive (or metallic sensing) pads 203 on the flexible substrate with a PDMS layer providing the elastic material 206. The conductive pads 203 were patterned using a milling machine (e.g., S100 by LPKF Inc.) on a flexible substrate with a thickness of, e.g., 10 mil. Other substrate thicknesses may be used such as, e.g., about 1 mil to about 100 mil. The sensitivity of the capacitive pressure sensors 109 can vary with pad size, so different sizes were fabricated. The dimensions of the conductive pads 203 from right to left are 3 mm \times 3 mm (203a), 4 mm \times 4 mm (203b), 5 mm \times 5 mm (203c), 6 mm \times 6 mm (203d), and 7 mm \times 7 mm (203e). The elastic material 206 can then be applied over the fabricated conductive pads 203. For example, a kit from Dow Corning may be used to apply a silicon elastomer coating of PDMS.

[0026] FIG. 4A shows the conductive pads 203 on the flexible substrate and PDMS layer lying flat. Since both the thin substrate and PDMS layer are flexible, the capacitive pad sensor 109 is deformable and can be fit in the uneven trench of the mouth guard 103. FIG. 4B shows an image of the conductive pads 203 on the flexible substrate and PDMS layer in a bent position. This flexibility makes the mouth guard 103 comfortable to wear.

[0027] The effect of the different conductive pad sizes is illustrated in FIG. 5A. The output of the conductive pads 203 was connected to an analog-to-digital converter (ADC) to digitize the data. FIG. 5A depicts the plots of the normalized ADC output with respect to the applied force for each conductive pad size: curve 503a for the 3 mm \times 3 mm pad 203a, curve 503b for the 4 mm \times 4 mm pad 203b, curve 503c for the

5 mm×5 mm pad **203c**, curve **503d** for the 6 mm×6 mm pad **203d**, and curve **503e** for the 7 mm×7 mm pad **203e**. As can be seen, the larger pad sizes exhibit a wider ADC output range. The effect of the thickness of the elastic material **206** was also examined. FIG. **5B** depicts the plots of the normalized ADC output with respect to the applied force for two different thicknesses of the PDMS layer: curve **506a** for 3 mm and curve **503b** for 4.5 mm.

[0028] Referring next to FIGS. **6A-6D**, shown are images of an example of a mouth guard **603** in accordance with various embodiments of the present disclosure. The mouth guard **603** of FIG. **6A** includes five capacitive pressure sensors **609** (5 mm×5 mm) distributed along a palatal surface of the mouth guard **603**. Other sensors such as, e.g., a temperature sensor and/or an inertia sensor may also be included. For example, one or more accelerometers and/or gyroscopes may be integrated into the mouth guard **603** to provide information regarding movement of the mouth guard **103** and/or the wearer. For instance, MEMS accelerometers and/or gyroscopes can provide six-axis information regarding, e.g., movement, tilt or shock. The mouth guard **603** also includes electronic processing circuitry **606** for sensing and/or wireless communications, and a power source **612** such as, e.g., a button cell battery. The capacitive pressure sensors **609**, electronic processing circuitry **606** and power source **612** were implemented on a flexible substrate and encased in PDMS using a professional dental molding process. Temperature, pH and inertia sensors may also be implemented on the flexible substrate and encased in PDMS. The mouth guard **603** was fitted to a user's upper teeth and palate for testing. The backside metal of the flexible substrate provides shielding of electrical noises from the human body. FIGS. **6B**, **6C**, and **6D** are images of the back, top, and front views of the mouth guard **603**, respectively.

[0029] The electronic processing circuitry **606** for sensing and/or wireless communications includes a transceiver, a microcontroller, one or more ADCs, and passive radio frequency (RF) components such as, e.g., an antenna, transmission lines, and a balun. Referring to FIG. **7**, shown is a graphical representation of an example of the SMS including, e.g., mouth guard **600** of FIGS. **6A-6D** or mouth guard **103** of FIG. **1**. For example, each capacitive pressure sensor **609** may be coupled to an ADC **703** (e.g., an AD7746 from Analog Device) to digitize the output data, which is then relayed for processing by a microcontroller **706**. The microcontroller **706** can provide the acquired sensor data to an external processing unit **106** through a transceiver **709** and antenna **712**. The microcontroller **706** and transceiver **709** may be implemented together as a microcontroller unit (MCU) such as, e.g., a CC2510 system on a chip (SoC) by Texas Instruments Inc., which includes a microcontroller and transceiver for more compact and power efficient system implementation. In some implementations, the electronic processing circuitry **606** may include memory to store sensor data for subsequent transmission to the external processing unit **106** and/or code or instructions that may be executed by the microcontroller **706**.

[0030] FIGS. **8A** and **8B** show front and back views of an implementation of the electronic processing circuitry **606**. The electronic processing circuitry **606** was fabricated on a flexible substrate (e.g., RO 3003, Rogers, Inc.) with a dimension of approximately 15 mm×15 mm. A temperature sensor in the chip of ADC **703** (e.g., CC1100, Texas Instruments Co.) may be used to provide an indication of whether a user is wearing the mouth guard, e.g., to address compliance issues.

Real-time temperature changes with a resolution of 0.1° C. and an accuracy of ±0.1° C. could be detected. The CC2510 chip contains an enhanced 8051 core microprocessor as well as an ISM band transceiver. Between the CC1100 ADC **703** and the CC2510 microcontroller **706**/transceiver **709**, an I2C communication protocol may be used. The digitized pressure information is modulated in the CC2510 microcontroller **706** and then transmitted to the free space wireless channel (or link) via a chip antenna **712**. Acceleration and/or gyroscopic sensors in a chip (not shown) may also be in communication with microcontroller **706** to provide indications of movement. In some implementations, at least a portion of the electronic processing circuitry **606** may be turned on and off using a magnetic reed switch. While the example of FIGS. **8A** and **8B** uses chip components for the concept proof, the circuit may be implemented using customized VLSI circuits. The whole electronic circuit and sensors may be realized in a size scale of a few millimeters or micrometers.

[0031] Power for the electronic processing circuitry **606** may be provided by a power source such as, e.g., a battery **118** (FIG. **1**) or **612** (FIG. **6A**). It may be desirable to avoid having to replace the battery. A wireless power delivery system may be used to supply power to a rechargeable battery through inductive coupling. The electronic processing circuitry **606** may be configured to regulate power delivery from an external source to recharge the battery. For example, a spiral antenna may be used for near field power coupling and bq500110 and bq51013 ICs from Texas Instruments may be used as the power transmitter and the receiver, respectively. Since the bq500110 and bq51013 ICs are highly integrated chips, nearly no peripherals are required on the receiver side for power collection, making it ideal for device size reduction.

[0032] Referring back to FIG. **7**, the external processing unit **106** includes an antenna **715** and transceiver **718** that receives the transmitted sensor information for analysis and processing by processing circuitry **721**. The SMS can utilize wireless telemetry (e.g., a transceiver that interfaces with a computer through a USB port) for self-monitoring and self-management of chronic stress using nocturnal bruxism as a stress indicator. The signal is transmitted over a wireless channel (or link) through a chip antenna **712** and received by antenna **715** and transceiver **718**. For example, a transceiver **718** and antenna **715** circuit including an MSP 430 IC and a CC2500 IC by Texas Instruments, Inc. may be provided in, e.g., a USB dongle shape as shown in FIG. **9**. The transceiver/antenna circuit may be configured to be plugged into the external processing unit **106** such as, e.g., a computing device (or PC) through a USB connector. Transmission between the mouth guard and the external processing unit **106** may be over, e.g., a 2.4 GHz communication link, a 403-405 MHz medical implant communication service (MICS) band, or other industry science medicine (ISM) bands including, e.g., 433 MHz, 915 MHz, and 5.8 GHz.

[0033] Communications between the mouth guard and external processing unit **106** may be carried out using a variety of communication protocols such as, e.g., SimpliCI™. For instance, a SimpliCI channel may be used for authentication, encryption, frequency hopping, etc. SimpliCI™ is a simple communication protocol especially designed for low cost and small scale network. Since it contains a device switch to change between sleep and active states, it is also known as a low power consuming protocol. The signal is transferred to a processing circuitry **721**, where it may be rendered and

displayed on a screen or display via a graphical user interface (GUI) 724 such as illustrated in FIG. 10. The data may then be displayed in a Windows GUI operating within the Windows API. Both real time and statistic data may be made available to the user through the GUI 724. The GUI 724 may also allow the user to configure operation of the electronic processing circuitry 606 of the mouth guard.

[0034] In various embodiments, the processing circuitry 721 is implemented as at least a portion of a microprocessor. The processing circuitry 721 may be implemented using one or more circuits, one or more microprocessors, application specific integrated circuits, dedicated hardware, digital signal processors, microcomputers, central processing units, field programmable gate arrays, programmable logic devices, state machines, or any combination thereof. In yet other embodiments, the processing circuitry 721 may include one or more software modules executable within one or more processing circuits. The processing circuitry 721 may further include memory configured to store instructions and/or code that causes the processing circuitry to execute analysis and processing functions.

[0035] Testing was performed by a user wearing the mouth guard of FIGS. 6A-6D in communication with an external processing unit 106 such as, e.g., a desktop personal computer. Operation was initially verified by recording a series of four bits. Data was collected by the SMS in real-time by the desktop personal computer. When active, data may be sampled for a predefined period such as, e.g., 0.1 sec, 0.5 sec, or 1 sec. The normalized ADC output curves 1103a-1103e are plotted in FIG. 11A for the five pressure sensors 609a-609e of FIG. 6A, respectively. The actuator 121 (FIG. 7) initiates sampling when pressure is applied and applies excitation when pressure is removed.

[0036] The electronic processing circuitry 606 may be programmed to maintain at least a portion of the circuitry in a sleep mode as long as the detected pressure level is below a predefined threshold. In this way, low pressure episodes are not recorded and data not transmitted. Once the detected pressure level exceeds the predefined threshold level, the electronic processing circuitry 606 switches to active mode to collect the pressure sensing data. When supra-threshold forces are present for a sufficiently long time, the force signal may be integrated over a specific time period. If the integral exceeds a threshold value, then the data may be stored in memory for later transmission or may be provided through real-time transmission. Since the average bruxing time per night is known to be approximately 10 minutes, use of a sleep mode may extend the system lifetime from one hour to six nights. In some implementations, multiple integrated data packets can be accumulated in memory before a batch transmission is initiated. For example, a brief transmission burst may be initiated for a few milliseconds for every minute during the active mode. Since the main power consumption in the SMS occurs during data transmission, batch data transmission can significantly reduce system power consumption. If the data transmission rate is reduced from 0.1 sec to 10 sec, the battery time may be extended by approximately 100 times.

[0037] FIG. 11B depicts a continuous mode test result, where curve 1106a corresponds to the normalized ADC output of pressure sensor 609a, curve 1106b corresponds to the normalized ADC output of pressure sensor 609b, and curve 1106c corresponds to the normalized ADC output of pressure sensor 609c. Between 2 to 4 seconds, when the left side of the

jaw clenches (episode 1), only pressure sensors 609a and 609b (curves 1106a and 1106b, respectively), which are in the proximity of the action, respond. Due to its remote location, pressure sensor 609c (curve 1106c) does not respond. Between 5 to 7 seconds, when the right side of the jaw clenches (episode 2), pressure sensors 609b and 609c (curves 1106b and 1106c, respectively) respond, whereas pressure sensor 609a (curve 1106a) does not respond. Between 8 to 11 seconds, when all sides of the jaws clench (episode 3), the action elicits a response from all three sensors. It should be noted that in episode 3, the biting force from all sides of the jaws is greater than that in episodes 1 and 2 with either side of the jaw, which is reflected in the larger magnitude recorded on the y-axis. The sensing data from pressure sensors 609d and 609e were measured as well, but not plotted for clarity.

[0038] When bruxing occurs during sleep, intervention by a clinician or therapist may not be readily available. An external processing unit 106 such as, e.g., a smart phone module or a personal computer with its superior computing power can compare the bruxing activity over an extended period of time and initiate a response only when recorded stress data are inconsistent with restful sleep or indicate potentially damaging force to the teeth or muscles. Intervention measures include the microprocessor triggering a mild electrical pulse to alert the wearer of bruxing or activating a drug delivery system to release a therapeutic agent, each of which may be integrated into the mouth guard. For instance, a compact coin type vibration motor (B1034, Yuesui Inc.), which is popularly used for a mobile phone vibrator, may be included for a hardware-based intervention approach in SMS. When bruxing occurs, mild vibration can be initiated to disturb the bruxing activity to prevent further dental or tissue damage. The frequency of the vibratory intervention may be calibrated and customized to the user. The SMS may be highly customizable according to patient needs.

[0039] Other forms of intervention may include initiating music therapy and/or activating a wake-up alarm. Once a response has been triggered to initiate music therapy, the external processing unit 106 (e.g., cell phone or linked computer) can determine from the patient's bruxing data whether the therapy has been effective. When bruxing activity fails to decline following the intervention, the external processing unit 106 may determine whether to administer additional therapy or alert a clinician. For example, a message may be sent to the clinician, who may then make contact with the user in response to the message. Captured data may also be transmitted to allow the clinician to evaluate the current conditions of the user. In this way, the clinician may be able to (a) remotely monitor the efficacy and progress of the user's self-management of stress, (b) establish a database to record the time course of stress levels of user on, e.g., a clinic server, (c) provide a basis for deciding whether follow-up sessions in the clinic should be recommended, (d) remotely change the automated therapeutic protocol for further personalization, and/or (e) intervene in person, e.g., via a phone call, if necessary.

[0040] As discussed, the system interfaces wirelessly with an external processing unit 106 such as, e.g., a mobile device or PC. For example, Bluetooth may be used for communications between SMS and a cell phone. Bluetooth offers a relatively large coverage range (about 100 meters for Class A device), high data rate (up to 2.1 Mb/s) and noise immunity by frequency-hopping spread spectrum (FHSS) technique. The electronic processing circuitry 606 of the mouth guard can also include an integrated Bluetooth chip. In this way, a

mobile smart phone may be used as the external processing unit **106** allowing for data acquisition device without a separate microprocessor or computer. An application operating on the cell (or smart) phone can control the activities of the SMS. For example, the application may store bruxing activity in the cell phone memory received from the mouth guard, analyze the bruxing activity by comparing the acquired data with preset threshold values, and/or initiate music therapy to improve relaxation if the threshold levels are exceeded. The collected data needs to be securely transferred through an encrypted or password protected channel.

[0041] The SMS may be used as a mHealth tool for chronic stress management. An external processing unit **106** such as, e.g., a smart phone, a smart watch (e.g., an Apple iWatch or Samsung Galaxy Gear), a PDA, a tablet (PC) device, a portable computer, or other mobile device may be used to continuously monitor health conditions for patients, realizing an “mHealth” (mobile health), a term used for the practice of medicine and public health supported by mobile devices. In some cases, applications such as, e.g., eMOCHA (electronic Mobile Open-source Comprehensive Health Application), can offer secure, highly flexible and adaptable mHealth app platforms, that may be utilized by the SMS with Android-supported devices. The curves of FIG. 11B demonstrate the ability of SMS to measure and quantify the intensity and duration of bruxism in real-time outside a research setting and for wirelessly transmitting data. The external processing unit **106** may execute appropriate applications (apps) to implement the mHealth monitoring system.

[0042] In some cases the mouth guard may be a retainer, which is a temporary device used to adjust and/or maintain alignment of teeth before and/or after dental braces. The integrated sensors can be used to monitor the use of the retainer by the wearer. For example, pressure and/or temperature sensors can be used to monitor how long the retainer has been worn and/or when the retainer can be removed based upon sensed force levels. Pressure and/or inertia sensors can also provide information regarding movement of the retainer while in use. The SMS can provide feedback to the wearer and/or others regarding use of the retainer.

[0043] Various examples are provided for smart mouth guards. In various aspects, among others, a diagnostic mouth guard is disclosed that includes a plurality of pressure sensors; and processing circuitry in communication with the plurality of pressure sensors, the processing circuitry configured to provide pressure sensor data to an external processing unit when located in an oral cavity. The processing circuitry can include an analog-to-digital converter (ADC), a microprocessor, and a transceiver embedded in the mouth guard. The transceiver can be configured to communicate with the external processing unit over a wireless channel. The diagnostic mouth guard can also include a temperature sensor, a pH sensor and/or an inertia sensor. The diagnostic mouth guard can also include an intervention feedback unit. The intervention feedback unit can include a vibration motor.

[0044] Various aspects of the present disclosure include a system comprising the diagnostic mouth guard and the external processing unit. In any one or more aspects of the system, the external processing unit can be configured to obtain the pressure sensor data from the processing circuitry of the diagnostic mouth guard. The external processing unit can be configured to process the obtained sensor data to determine a condition of bruxism. The external processing unit can be configured to initiate an intervention in response to the deter-

mination of the condition of bruxism. The intervention can be an initiation of music therapy and/or an initiation of feedback provided by the diagnostic mouth guard. The feedback provided by the diagnostic mouth guard can be a vibration. In any one or more aspects of the system, the external processing unit can be configured to provide an indication of the condition of bruxism through a graphical user interface (GUI).

[0045] In any one or more aspects of the system, the external processing unit can be a smart phone, a smart watch, a personal computer or a tablet computer. The smart phone, smart watch, personal computer or tablet computer can be configured to implement an “mHealth” (mobile-health) monitoring system. In any one or more aspects of the system, the external processing unit can be a cell phone configured to implement an “mHealth” (mobile-health) monitoring system. In any one or more aspects, the smart mouth guard can be a retainer.

[0046] It should be emphasized that the above-described embodiments of the present disclosure are merely possible examples of implementations set forth for a clear understanding of the principles of the disclosure. Many variations and modifications may be made to the above-described embodiment(s) without departing substantially from the spirit and principles of the disclosure. All such modifications and variations are intended to be included herein within the scope of this disclosure and protected by the following claims.

[0047] It should be noted that ratios, concentrations, amounts, and other numerical data may be expressed herein in a range format. It is to be understood that such a range format is used for convenience and brevity, and thus, should be interpreted in a flexible manner to include not only the numerical values explicitly recited as the limits of the range, but also to include all the individual numerical values or sub-ranges encompassed within that range as if each numerical value and sub-range is explicitly recited. To illustrate, a concentration range of “about 0.1% to about 5%” should be interpreted to include not only the explicitly recited concentration of about 0.1 wt % to about 5 wt %, but also include individual concentrations (e.g., 1%, 2%, 3%, and 4%) and the sub-ranges (e.g., 0.5%, 1.1%, 2.2%, 3.3%, and 4.4%) within the indicated range. The term “about” can include traditional rounding according to significant figures of numerical values. In addition, the phrase “about ‘x’ to ‘y’” includes “about ‘x’ to about ‘y’”.

1. A diagnostic mouth guard, comprising:
 - a plurality of pressure sensors; and
 - processing circuitry in communication with the plurality of pressure sensors, the processing circuitry configured to provide pressure sensor data to an external processing unit when located in an oral cavity.
2. The diagnostic mouth guard of claim 1, wherein the processing circuitry includes an analog-to-digital converter (ADC), a microprocessor, and a transceiver embedded in the mouth guard.
3. The diagnostic mouth guard of claim 2, wherein the transceiver is configured to communicate with the external processing unit over a wireless channel.
4. The diagnostic mouth guard of claim 1, further comprising a temperature sensor.
5. The diagnostic mouth guard of claim 1, further comprising an intervention feedback unit.
6. The diagnostic mouth guard of claim 5, wherein the intervention feedback unit comprises a vibration motor.

7. The diagnostic mouth guard of claim 1, further comprising an inertia sensor comprising an accelerometer or a gyroscope.

8. A system, comprising:
the diagnostic mouth guard of claim 1; and
the external processing unit.

9. The system of claim 8, wherein the external processing unit is configured to obtain the pressure sensor data from the processing circuitry of the diagnostic mouth guard.

10. The system of claim 9, wherein the external processing unit is configured to process the obtained sensor data to determine a condition of bruxism.

11. The system of claim 10, wherein the external processing unit is configured to initiate an intervention in response to the determination of the condition of bruxism.

12. The system of claim 11, wherein the intervention is an initiation of music therapy.

13. The system of claim 11, wherein the intervention is an initiation of feedback provided by the diagnostic mouth guard.

14. The system of claim 13, wherein the feedback provided by the diagnostic mouth guard is a vibration.

15. The system of claim 10, wherein the external processing unit is further configured to provide an indication of the condition of bruxism through a graphical user interface (GUI).

16. The system of claim 8, wherein the external processing unit is a smart phone or a smart watch.

17. The system of claim 8, wherein the external processing unit is a personal computer.

18. The system of claim 8, wherein the external processing unit is a tablet computer.

19. The system of claim 18, wherein the tablet computer is configured to implement an "mHealth" (mobile-health) monitoring system.

20. The system of claim 8, wherein the external processing unit is a cell phone or a smart watch configured to implement an "mHealth" (mobile-health) monitoring system.

* * * * *

专利名称(译)	智能诊断口保护系统		
公开(公告)号	US20150305671A1	公开(公告)日	2015-10-29
申请号	US14/760641	申请日	2014-01-14
[标]申请(专利权)人(译)	佛罗里达大学研究基金会有限公司		
申请(专利权)人(译)	佛罗里达州研究基金会, Inc.的大学.		
当前申请(专利权)人(译)	佛罗里达州研究基金会, Inc.的大学.		
[标]发明人	YOON YONG KYU CHENG XIAOYU KIM GLORIA JUNG A WONG FONG		
发明人	YOON, YONG-KYU CHENG, XIAOYU KIM, GLORIA JUNG-A WONG, FONG		
IPC分类号	A61B5/00 A61B5/01 A61M21/02 A61F5/56		
CPC分类号	A61B5/4557 A61M2205/3303 A61B5/682 A61B5/01 A61B5/0008 A61B5/486 A61B5/7455 A61B5/7282 A61M21/02 A61B5/742 A61B5/7475 A61B5/681 A61B5/6898 A61B5/4836 A61F2005/563 A61B2562 /0219 A61M2021/0027 A61F5/566 A61B5/228 A61B5/4839		
优先权	61/752142 2013-01-14 US		
其他公开文献	US10517525		
外部链接	Espacenet USPTO		

摘要(译)

提供了用于智能护嘴的各种示例，用于诊断，量化和/或管理例如磨牙症。在一个示例中，诊断护口器包括多个压力传感器和处理电路，其配置成当位于口腔中将压力传感器数据提供给外部处理单元。诊断护口器还可包括温度，pH和/或惯性传感器。在另一个例子中，系统包括诊断护口罩和外部处理单元，例如智能电话，桌子或计算机。诊断护口罩可以通过无线信道与外部处理单元通信。

