



US010045733B2

(12) **United States Patent**
Takakura et al.

(10) **Patent No.:** **US 10,045,733 B2**
(45) **Date of Patent:** **Aug. 14, 2018**

(54) **SLEEP SENSOR**

(71) Applicant: **TDK Corporation**, Minato-ku, Tokyo (JP)

(72) Inventors: **Junya Takakura**, Kanagawa (JP);
Kanako Nakayama, Tokyo (JP);
Yasunobu Yamauchi, Kanagawa (JP)

(73) Assignee: **TDK CORPORATION**, Tokyo (JP)

(*) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 202 days.

(21) Appl. No.: **14/749,106**

(22) Filed: **Jun. 24, 2015**

(65) **Prior Publication Data**

US 2015/0374284 A1 Dec. 31, 2015

(30) **Foreign Application Priority Data**

Jun. 25, 2014 (JP) 2014-130290

(51) **Int. Cl.**
A61B 5/08 (2006.01)
A61B 5/00 (2006.01)
(Continued)

(52) **U.S. Cl.**
CPC **A61B 5/4818** (2013.01); **A61B 5/0826** (2013.01); **A61B 5/1116** (2013.01);
(Continued)

(58) **Field of Classification Search**
CPC ... A61B 5/4806; A61B 5/4818; A61B 5/7285;
A61B 5/7278; A61B 5/1116;
(Continued)

(56) **References Cited**

U.S. PATENT DOCUMENTS

6,356,203 B1 *	3/2002	Halleck		A61B 5/1117
				200/61.45 R
2009/0062628 A1 *	3/2009	Yamamoto		A61B 5/08
				600/301
2009/0062828 A1	3/2009	Yamamoto et al.		
2011/0066042 A1 *	3/2011	Pandia		A61B 5/029
				600/484

(Continued)

FOREIGN PATENT DOCUMENTS

JP	2001-190503 A	7/2001
JP	2006-247374	9/2006
JP	2013-236925 A	11/2013

OTHER PUBLICATIONS

Richard, Wietske, et al. "The role of sleep position in obstructive sleep apnea syndrome." *European Archives of Oto-Rhino-Laryngology and Head & Neck* 263.10 (2006): 946-950.*

(Continued)

Primary Examiner — Navin Natnithithadha

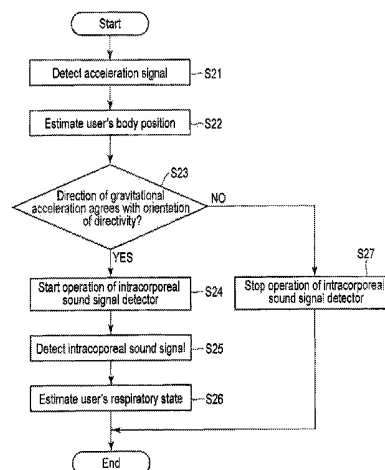
Assistant Examiner — Andrey Shostak

(74) *Attorney, Agent, or Firm* — Oliff PLC

(57) **ABSTRACT**

According to one embodiment, a sleep sensor which is attached to a user who is sleeping when it is to be used is provided. The sleep sensor includes a first detector, an estimation module, a second detector and a control module. The first detector is configured to detect an acceleration signal representing acceleration that is obtained from the sleep sensor. The estimation module is configured to estimate the user's body position based on the detected acceleration signal. The second detector is configured to detect a signal for estimating a state other than the user's body position. The control module is configured to operate the second detector when the estimated user's body position is at least one of predefined body positions.

1 Claim, 7 Drawing Sheets



- (51) **Int. Cl.**
A61B 5/11 (2006.01)
A61B 7/00 (2006.01)
- (52) **U.S. Cl.**
CPC *A61B 5/6823* (2013.01); *A61B 5/7278*
(2013.01); *A61B 5/7285* (2013.01); *A61B*
7/003 (2013.01); *A61B 2560/0412* (2013.01);
A61B 2562/0204 (2013.01); *A61B 2562/0219*
(2013.01)
- (58) **Field of Classification Search**
CPC ... A61B 5/4815; A61B 5/6823; A61B 5/0205;
A61B 5/0402; A61B 5/113; A61B 5/024;
A61B 5/02055; A61B 5/08; A61B
5/0245; A61B 5/0826; A61B 7/003; A61B
2562/0204; A61B 2562/0219; A61B
2560/0412
See application file for complete search history.

(56) **References Cited**

U.S. PATENT DOCUMENTS

2011/0137209 A1* 6/2011 Lahiji A61B 7/026
600/586
2013/0281883 A1 10/2013 Nishida

OTHER PUBLICATIONS

English-language extended European search report by the European
Patent Office in counterpart foreign Application No. 15168923.9,
dated Nov. 23, 2015, 7 pages.

* cited by examiner

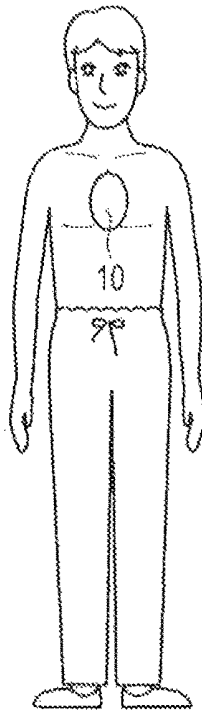


FIG. 1

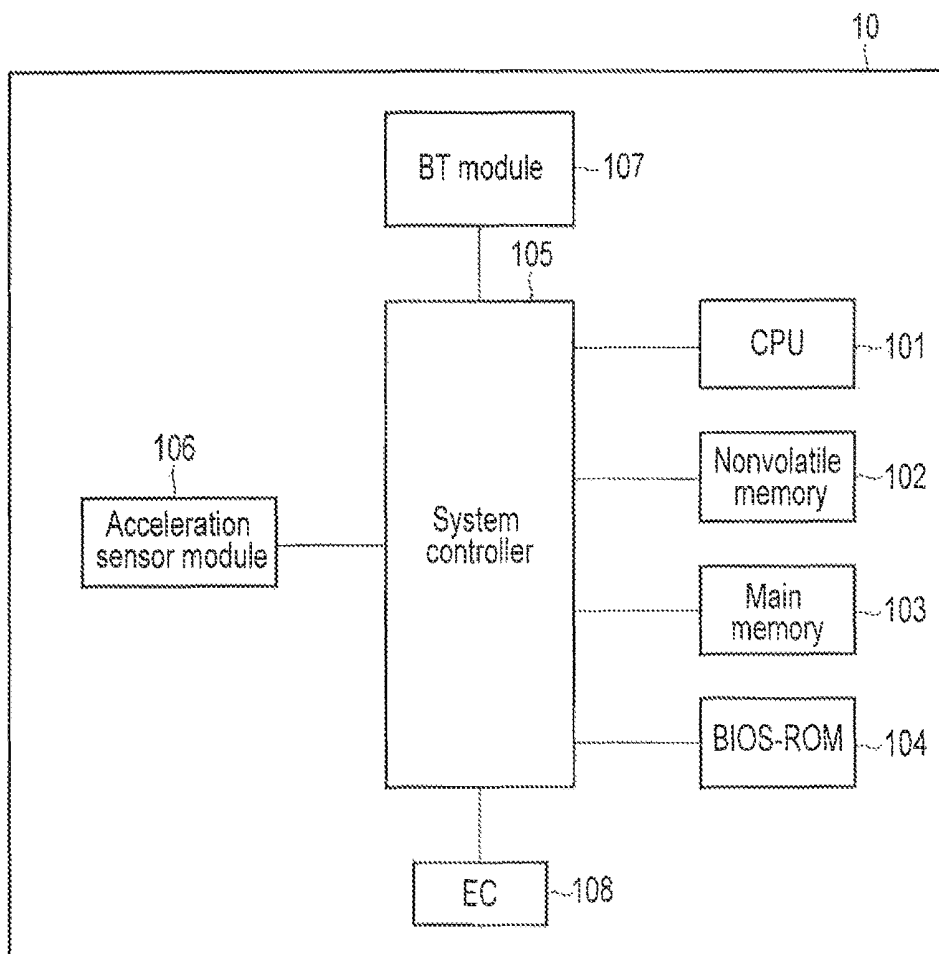


FIG. 2

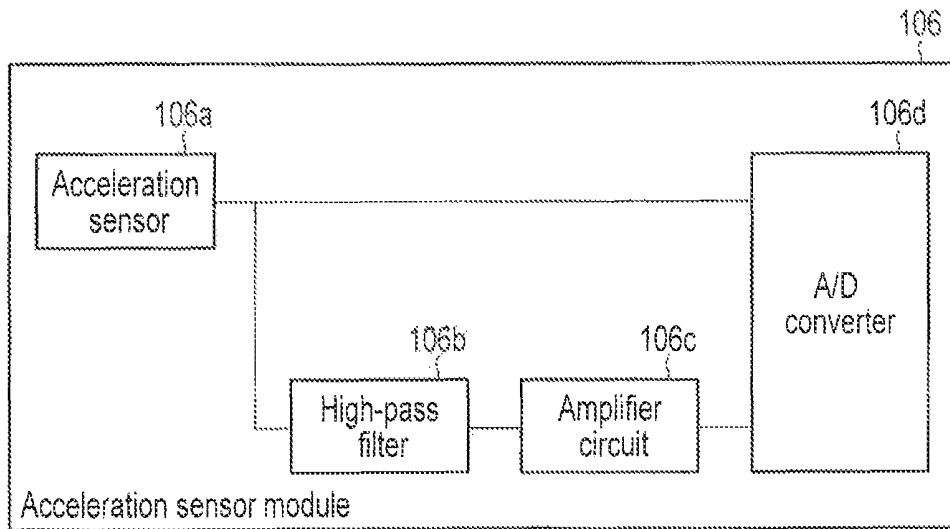


FIG. 3

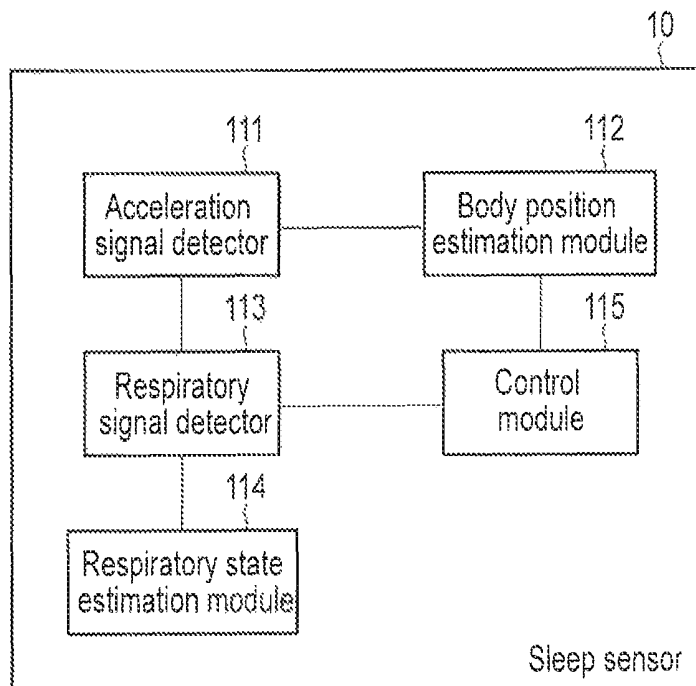


FIG. 4

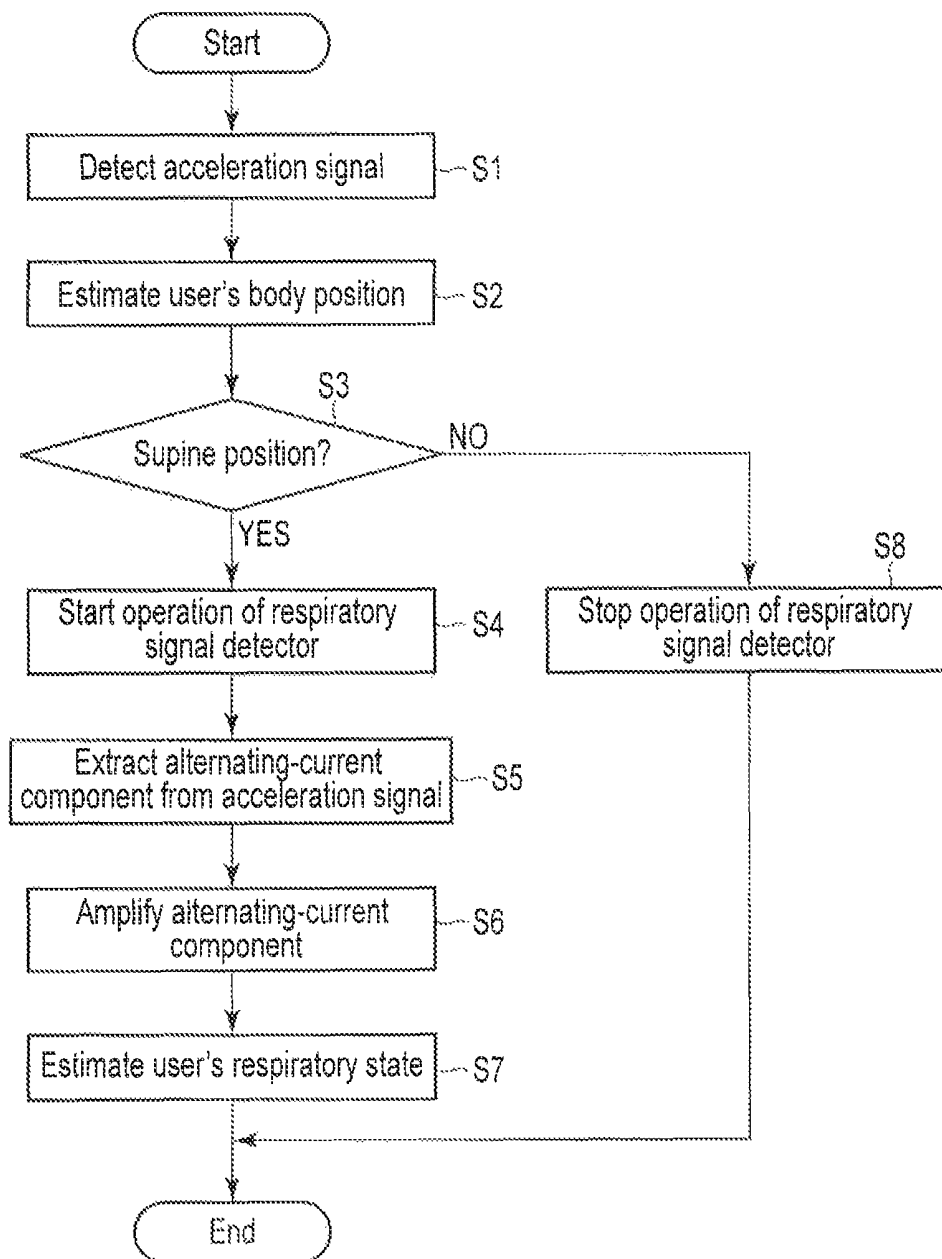


FIG. 5

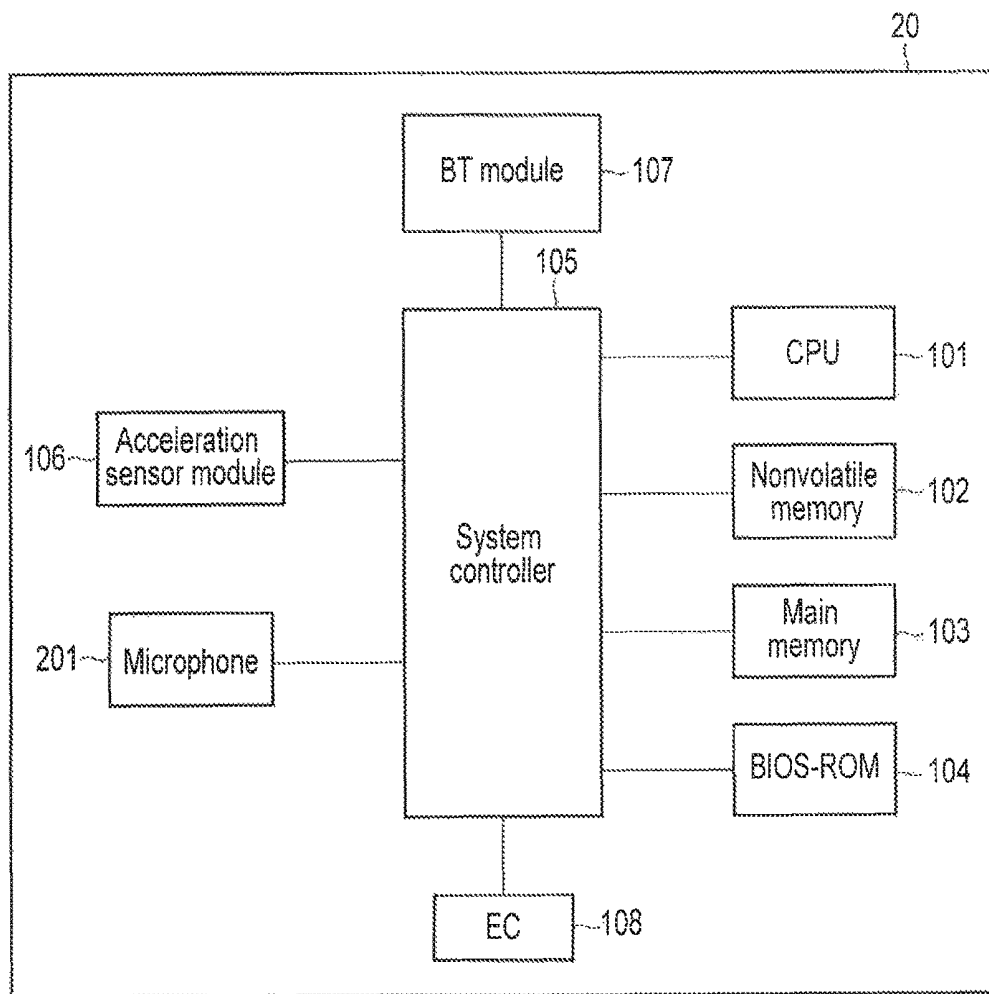
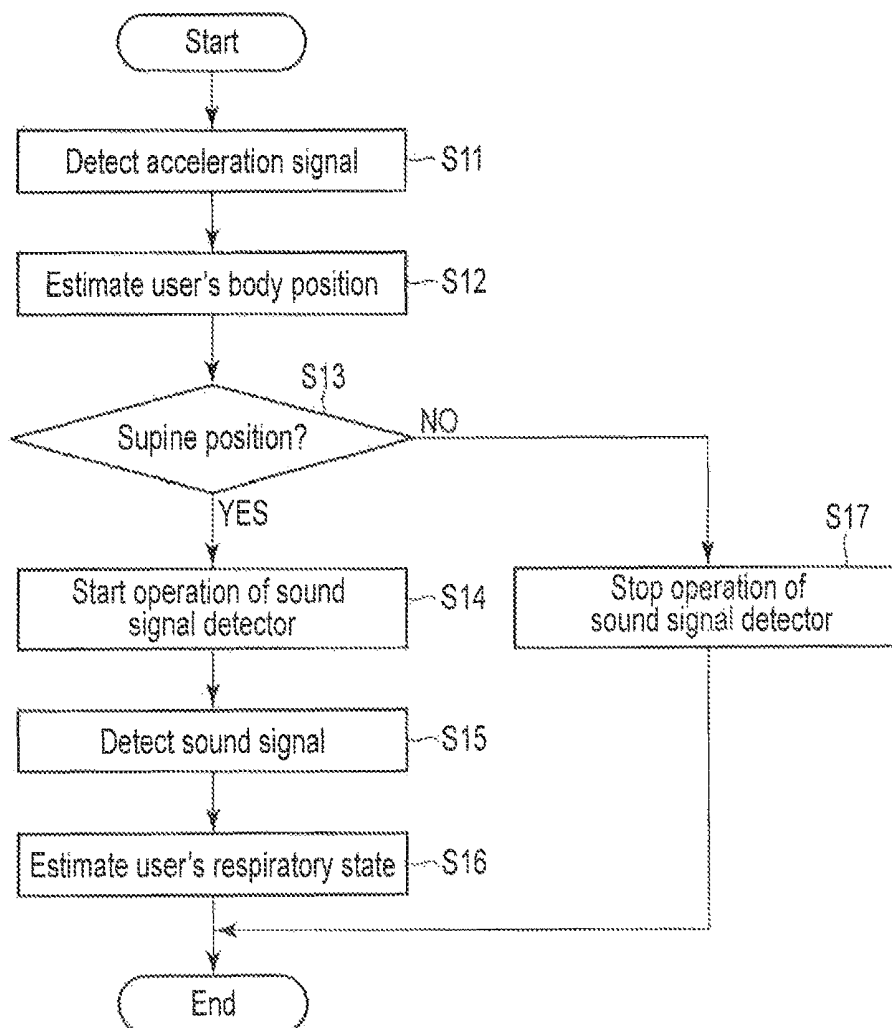
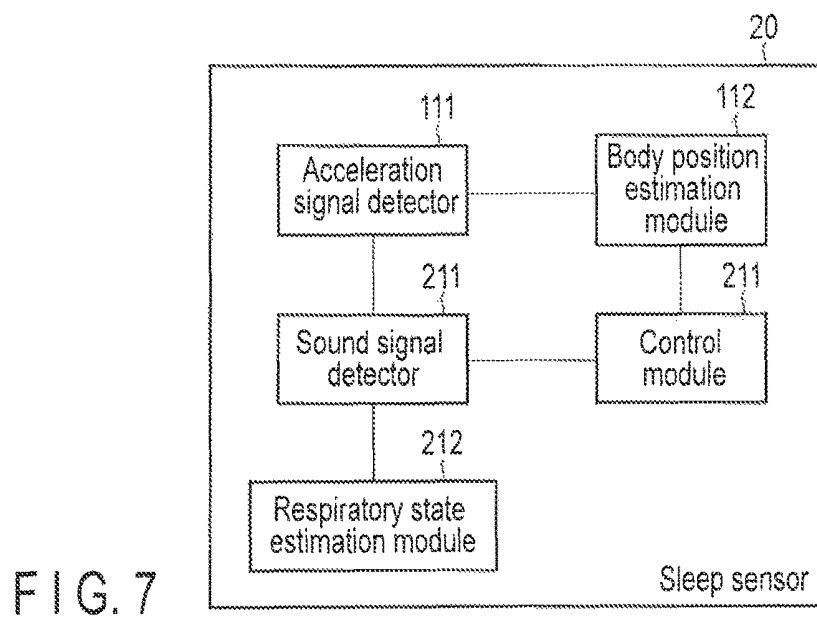


FIG. 6



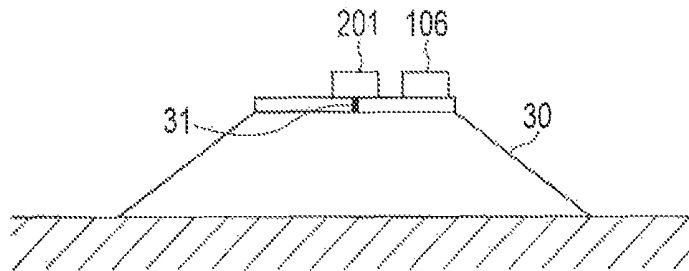


FIG. 9

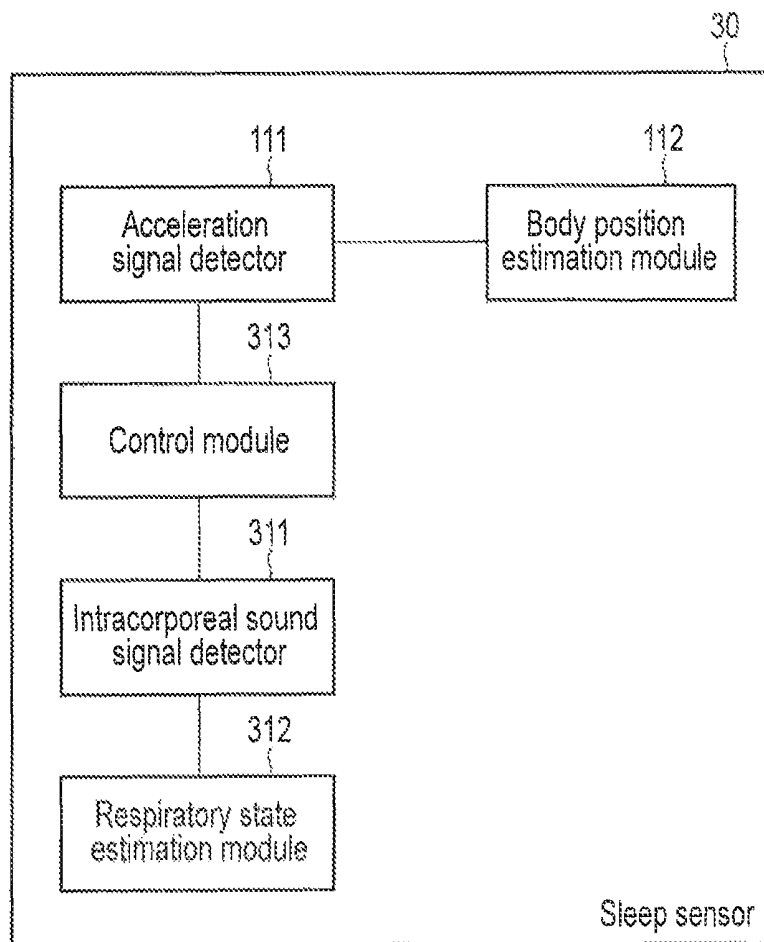


FIG. 10

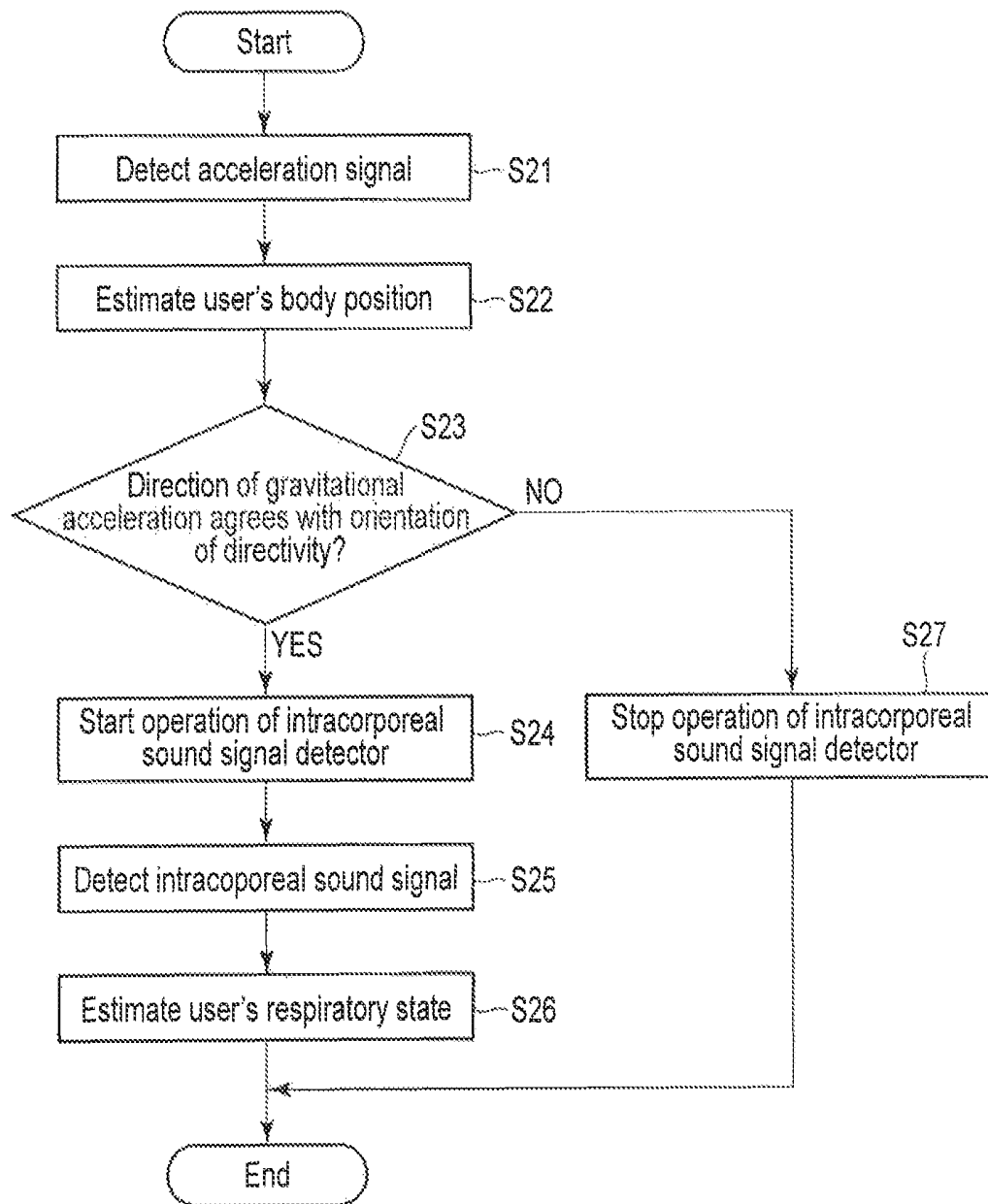


FIG. 11

1

SLEEP SENSOR

CROSS-REFERENCE TO RELATED
APPLICATIONS

This application is based upon and claims the benefit of priority from Japanese Patent Application No. 2014-130290, filed Jun. 25, 2014, the entire contents of which are incorporated herein by reference.

FIELD

Embodiments described herein relate generally to a sleep sensor for estimating a state of a user during sleep.

BACKGROUND

Generally, in order to carry out a diagnosis of sleep apnea syndrome, for example, the user's state during sleep (hereinafter referred to as a sleep state) is estimated by using a body position sensor or a snore sensor, etc.

In this case, the body position sensor is attached to, for example, the user's chest, and the snore sensor is attached to, for example, the user's throat. Sleeping with a plurality of sensors separately attached at different parts of the body is very troublesome for the user.

Hence, recently, a sleep sensor (device) including a plurality of sensors to be used for estimating the user's sleep state has been developed. According to such a sleep sensor, not only the user's body position and respiratory state during sleep, but also other conditions such as electrocardiographic activity, pulse waves, and body temperature can be estimated. Also, since it becomes unnecessary to attach a plurality of sensors separately as mentioned above, the burden on the user can be reduced.

Incidentally, the above-mentioned sleep sensor is often driven, by power supplied from a battery. In this situation, the sleep sensor must be driven by power supplied from the battery alone for a long time in order to estimate the user's sleep state as described above.

However, since the power supplied from the battery is limited, a mechanism for achieving power-saving in order to realize long-time driving of the sleep sensor including a plurality of sensors is desired.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is an illustration showing an example of usage of a sleep sensor according to a first embodiment;

FIG. 2 is a diagram showing a system configuration of the sleep sensor shown in FIG. 1;

FIG. 3 is a diagram for describing a configuration of an acceleration sensor module shown in FIG. 2;

FIG. 4 is a block diagram showing mainly a functional configuration of the sleep sensor according to the present embodiment;

FIG. 5 is a flowchart showing a processing procedure when the sleep sensor according to the present embodiment estimates the user's sleep state;

FIG. 6 is a diagram showing a system configuration of a sleep sensor according to a second embodiment;

FIG. 7 is a block diagram showing mainly a functional configuration of the sleep sensor according to the present embodiment;

FIG. 8 is a flowchart showing a processing procedure when the sleep sensor according to the present embodiment estimates the user's sleep state;

2

FIG. 9 is an illustration for describing the shape of a sleep sensor according to a third embodiment;

FIG. 10 is a block diagram showing mainly a functional configuration of the sleep sensor according to the present embodiment; and

FIG. 11 is a flowchart showing a processing procedure when the sleep sensor according to the present embodiment estimates the user's sleep state.

DETAILED DESCRIPTION

Various embodiments will be described hereinafter with reference to the accompanying drawings.

In general, according to one embodiment, a sleep sensor which is attached to a user who is sleeping when it is to be used is provided. The sleep sensor includes a first detector, an estimation module, a second detector and a control module. The first detector is configured to detect an acceleration signal representing acceleration that is obtained from the sleep sensor. The estimation module is configured to estimate the user's body position based on the detected acceleration signal. The second detector is configured to detect a signal for estimating a state other than the user's body position. The control module is configured to operate the second detector when the estimated user's body position is at least one of predefined body positions.

First Embodiment

FIG. 1 shows an example of usage of a sleep sensor (device) according to a first embodiment. A sleep sensor 10 shown in FIG. 1 is a small, light, and thin device which is used for estimating the user's state during sleep (which is hereinafter referred to as a sleep state). By using double-faced adhesive tape having adhesiveness or a gel pad, etc., an attachment surface of the sleep sensor 10 is stuck to the chest of the user who is sleeping when it is to be used. The sleep sensor 10 has a shape which is close to an oval or a rectangle, for example, to allow the sleep sensor 10 to be easily attached near the central part of the chest.

Note that the user's sleep state estimated by the sleep sensor 10 includes, for example, the user's body position (orientation or posture of the body), and respiratory state during sleep.

FIG. 2 is a diagram showing a system configuration of the sleep sensor 10 shown in FIG. 1. As shown in FIG. 2, the sleep sensor 10 includes a CPU 101, a nonvolatile memory 102, a main memory 103, a BIOS-ROM 104, a system controller 105, an acceleration sensor module 106, a BT module 107, an EC 108, etc.

The CPU 101 is a processor for controlling the operation of each component in the sleep sensor 10. The CPU 101 executes various kinds of software loaded into the main memory 103 from the nonvolatile memory 102, which is a storage device.

The CPU 101 executes a Basic Input/Output System (BIOS) stored in the BIOS-ROM 104. The BIOS is a program for hardware control.

The system controller 105 is a bridge device for connecting between the CPU 101 and each component. The CPU 101, the nonvolatile memory 102, the main memory 103, the BIOS-ROM 104, the acceleration sensor module 106, the BT module 107, the EC 108, etc. are connected to the system controller 105.

The acceleration sensor module 106 includes an acceleration sensor capable of sensing an acceleration signal, and is a module used for estimating the user's body position and

respiratory state of during sleep. A configuration of the acceleration sensor module **106** will be described later.

The BT module **107** is a module configured to execute wireless communication with a Bluetooth-enabled device by using Bluetooth (registered trademark). The Bluetooth-enabled device includes, for example, a smartphone, a tablet computer, and a personal computer (PC).

The EC **108** is a power management controller for executing power management of the sleep sensor **10**.

Note that several kinds of sensors capable of sensing, for example, the electrocardiographic activity, pulse waves, and body temperature may be provided in the sleep sensor **10** of the present embodiment, other than the above-mentioned acceleration sensor, although this is not illustrated in FIG. 2.

As can be seen, a plurality of sensors are provided within a single housing of the sleep sensor **10**. Here, since analog front ends of the plurality of sensors have different specifications depending on the type of sensor, satisfying both the flexibility and high-performance is required, which may lead to an increase in size. However, in the present embodiment, since a plurality of analog front ends and the CPU **101**, etc. are integrated on a single chip by using psuedo-SoC technology, a module of several millimeters square is realized. Note that the psuedo-SoC technology is one which satisfies both size reduction equivalent to an SoC and a degree of design freedom equivalent to an SiP by integrating parts on a wafer. By connecting an antenna and only a few peripheral parts such as a battery to the module, the sleep sensor **10** which is small, light (ten-odd grams or so), and thin (several millimeters or so) can be realized. Note that while it has been described size reduction of the sleep sensor **10** is realized by using the psuedo-SoC technology, the size reduction can also be realized by using an LSI, for example.

With reference to FIG. 3, the configuration of the acceleration sensor module **106** shown in FIG. 2 will be described. As shown in FIG. 3, the acceleration sensor module **106** includes an acceleration sensor **106a**, a high-pass filter **106b**, an amplifier circuit **106c**, an A/D converter **106d**, etc.

The acceleration sensor **106a** is a sensor for sensing an acceleration signal representing acceleration that acts on the sleep sensor **10**. It is assumed that the acceleration sensor **106a** is a triaxial acceleration sensor (a three-dimensional acceleration sensor) capable of sensing the acceleration signal in each of the directions of, for example, three orthogonal axes (the x-axis, the y-axis, and the z-axis). Also, the acceleration signal sensed (output) by the acceleration sensor **106a** are an analog signal.

Note that while the sleep sensor **10** has, for example, an oval shape as described above, (the acceleration signal produced in accordance with) an vibratory motion is sometimes hard to be sensed near the center of the sleep sensor **10**. Accordingly, in order to more accurately sense the acceleration signal, the acceleration sensor **106a** is arranged at a position which is deviated from the center of the sleep sensor **10**, for example.

The high-pass filter **106b** extracts an alternating-current component of the acceleration signal from the acceleration signal sensed by the acceleration sensor **106a**.

The amplifier circuit (analog circuit) **106c** amplifies the alternating-current component extracted by the high-pass filter **106b**.

The A/D converter **106d** converts the acceleration signal (an analog signal) sensed by the acceleration sensor **106a** into a digital signal. Also, the A/D converter **106d** converts the alternating-current component of the acceleration signal amplified by the amplifier circuit **106c** into a digital signal.

FIG. 4 is a block diagram showing mainly a functional configuration of the sleep sensor **10** according to the present embodiment. As shown in FIG. 4, the sleep sensor **10** includes an acceleration signal detector **111**, a body position estimation module **112**, a respiratory signal detector **113**, a respiratory state estimation module **114**, and a control module **115**.

The acceleration signal detector **111** is a functional module which is realized by the acceleration sensor **106a** described above, and detects the acceleration signal by using the acceleration sensor **106a**. That is, the acceleration signal detector **111** detect an acceleration signal representing acceleration that is obtained from the sleep sensor **10**. The acceleration signal detected by the acceleration signal detector **111** includes a direct-current component mainly representing gravitational acceleration, and an alternating-current component mainly representing acceleration which is produced by the user's state (for example, the respiratory state).

The body position estimation module **112** estimates the user's body position during sleep based on the acceleration signal detected by the acceleration signal detector **111**. Note that the user's body position estimated by the body position estimation module **112** includes positions such as a supine position, a prone position, and a lateral position.

The respiratory signal detector **113** is a functional module which is realized by the high-pass filter **106b** and the amplifier circuit **106c**. The respiratory signal detector **113** cuts the direct-current component of the acceleration signal detected by the acceleration signal detector **111** in the high-pass filter **106b**, and extracts the alternating-current component (a high-frequency component) of the acceleration signal. Also, the respiratory signal detector **113** amplifies the extracted alternating current component of the acceleration signal by using the amplifier circuit **106c**. The respiratory signal detector **113** thereby detects the amplified alternating-current component of the acceleration signal as a signal for estimating the state other than the user's body position (here, the user's respiratory state). In the following descriptions, the signal detected by the respiratory signal detector **113** (i.e., the amplified alternating-current component of the acceleration signal) will be referred to as a respiratory signal.

The respiratory state estimation module **114** estimates the user's respiratory state during sleep based on a respiratory signal detected by the respiratory signal detector **113**. Note that the user's respiratory state estimated by the respiratory state estimation module **114** includes, for example, presence or absence of a symptom of snoring during sleep.

The control module **115** controls the operation of the respiratory signal detector **113**. Specifically, the control module **115** executes the control to operate the respiratory signal detector **113** when the user's body position estimated by the body position estimation module **112** is at least one of predefined body positions (for example, the supine position, the prone position and so on).

The body position estimation module **112** and the respiratory state estimation module **114** are functional modules which are realized when the CPU **101** executes predetermined software (program). Further, the control module **115** is a functional module which is realized by, for example, the system controller **105**.

Next, referring to the flowchart of FIG. 5, a processing procedure when the sleep sensor **10** according to the present embodiment estimates the user's sleep state (the body position and the respiratory state) will be described.

Firstly, the acceleration signal detector **111** detects an acceleration signal by using the acceleration sensor **106a**

(step S1). Note that the acceleration signal detected by the acceleration signal detector **111** is converted into a digital signal in the A/D converter **106d**, and handed over to the body position estimation module **112**.

The body position estimation module **112** estimates the user's body position during sleep based on the acceleration signal which has been converted into the digital signal in the A/D converter **106d** (step S2).

Here, the estimation processing of the user's body position will be specifically described. Firstly, while the acceleration signal detected by the acceleration signal detector **111** includes a direct-current component (gravitational acceleration) and an alternating-current component (acceleration which is produced by the respiratory state, etc.) as described above, the acceleration sensor **106a** in the present embodiment is a triaxial acceleration sensor. Accordingly, a direction of gravitational acceleration with respect to the sleep sensor **10** can be calculated from (the direct-current component of) the acceleration signal in each axial direction sensed by the acceleration sensor **106a**. The user's body position is estimated based on the direction of the gravitational acceleration with respect to the sleep sensor **10** which has been thus calculated.

More specifically, with reference to the attachment surface of the sleep sensor **10**, axes horizontal to the attachment surface and orthogonal to each other are defined as the x-axis and the y-axis, and an axis orthogonal to the x-axis and the y-axis (i.e., the axis normal to the attachment surface) is defined as the z-axis. When the sleep sensor **10** is attached to the user's chest, as shown in FIG. 1, the x-axis corresponds to a transverse axis relative to the user's body (i.e., the direction of right and left of the body), the y-axis corresponds to a longitudinal axis relative to the user's body (i.e., the direction of head to toe of the body), and the z-axis corresponds to a front-to-back axis relative to the user.

In this case, when the direction of the gravitational acceleration with respect to the sleep sensor **10** is the back direction of the user in the z-axis (that is, backward to the user), it is estimated that the user's body position is the supine position. Meanwhile, when the direction of the gravitational acceleration with respect to the sleep sensor **10** is the front direction of the user in the z-axis (that is, forward to the user), it is estimated that the user's body position is the prone position. Also, when the direction of the gravitational acceleration with respect to the sleep sensor **10** is the x-direction (that is, right or left to the user), it is estimated that the user's body position is the lateral position.

When the user's body position is estimated in the above-described step S2, it is determined whether the user's body position, which has been estimated is the supine position (step S3).

When it has been determined that the user's body position is the supine position (YES in step S3), the control module **115** executes the control of starting the operation of the respiratory signal, detector **113** (step S4). In this case, the control module **115** powers on the respiratory signal detector **113** (that is, the high-pass filter **106b** and the amplifier circuit **106c**). Accordingly, the respiratory signal detector **113** is able to detect a respiratory signal.

In this case, the respiratory signal detector **113** extracts, from the acceleration signal detected by the acceleration signal detector **111** in step S1, an alternating-current component of the acceleration signal, by using the high-pass filter **106b** (step S5).

Here, the A/D converter **106d** according to the present embodiment needs to perform A/D conversion for both of (the direct-current component of) the acceleration signal

detected by the acceleration signal detector **111** and the alternating-current component of the acceleration signal, in order so estimate the user's body position and respiratory state. In this case, the amplitude of the alternating-current component of the acceleration signal is extremely small as compared to that of the acceleration signal. More specifically, while detecting an acceleration signal within the range of ± 1 G is necessary to estimate the body position, the magnitude of the alternating-current component of the acceleration signal detected for estimating the respiratory state is, for example, several milliG or less. In contrast, a resolution of the A/D converter **106d** which can be mounted on the sleep sensor **10** is generally 8 to 12 bits or so, for example.

That is, the alternating-current component of the acceleration signal extracted by using the high-pass filter **106b** cannot be processed by the A/D converter **106d** as it is. Hence, the respiratory signal detector **113** amplifies the extracted alternating-current component, of the acceleration signal by using the amplifier circuit **106c** (step S6). An amplification rate of the alternating-current component of the acceleration signal in this case is assumed to be adjusted in accordance with a dynamic range of the A/D converter **106d** such that the alternating-current component can be processed even by the resolution of the A/D converter **106d**.

The alternating-current component of the acceleration signal amplified by the respiratory signal detector **113** (that is, the respiratory signal detected by the respiratory signal detector **113**) is converted into a digital signal by the A/D converter **106d**, and handed over to the respiratory state estimation module **114**.

The respiratory state estimation module **114** estimates presence or absence of a symptom of snoring, for example, as the user's respiratory state during sleep, on the basis of the respiratory signal converted into the digital signal in the A/D converter **106d** (step S7). In this case, the respiratory state estimation module **114** estimates the presence or absence of a symptom of snoring based on a feature amount calculated on the basis of, for example, the respiratory signal.

Meanwhile, when it is determined that the user's body position is not the supine position in the above step S3 (NO in step S3), the control module **115** executes the control of stopping the operation of the respiratory signal detector **113** (step S8). In this case, the control module **115** turns off power of the respiratory signal detector **113** (that is, the high-pass filter **106b** and the amplifier circuit **106c**). When this is carried out, since the respiratory signal detector **113** cannot detect a respiratory signal, the processing of the sleep sensor **10** is terminated.

It should be noted that the result of estimation of the user's body position in the above step S2, and the result of estimation of the user's respiratory state in step S7 are transmitted to an external Bluetooth-enabled device (a smartphone, a tablet computer, a PC, etc.) via the above-described BT module **107**, and provided (presented) to a user, for example.

Note that while it has been described that each result of estimation is transmitted to a Bluetooth-enabled device, it is possible to adopt a structure in which the result of estimation is transmitted to an external server apparatus, etc., which functions as a cloud server that provides, for example, cloud computing service via a wireless LAN, etc., and stored in the server apparatus. Also, the result of estimation may be stored within the sleep sensor **10**.

As described above, in the present embodiment, an acceleration signal representing acceleration that is obtained from the sleep sensor **10** is detected, and the user's body position is estimated based on the detected acceleration signal (gravi-

tational acceleration). Further, in the present embodiment, a respiratory signal (an alternating-current component of the acceleration signal) is detected from the detected acceleration signal, and the user's respiratory state (presence or absence of a symptom of snoring) is estimated based on the detected respiratory signal. Also, in the present embodiment, the control to operate the respiratory signal detector **113** is executed when the estimated user's body position is a predefined body position (for example, the supine position). That is, in the present embodiment, control on a detection operation of a signal for estimating other states can be varied in accordance with a result of estimation of the user's body position.

Consequently, in the present embodiment, since the respiratory signal is detected (that is, the user's respiratory state is estimated) only when the user's body position is the supine position in terms of the fact that, for example, snoring is likely to occur in the supine position, it becomes possible to reduce the power consumption (that is, achieve power saving) when the user's body position is a position other than the supine position.

Also, in the present embodiment, since the user's respiratory state is estimated by using the alternating-current component extracted from the acceleration signal detected by the acceleration signal detector **111**, it is unnecessary so provide, a sensor for estimating the user's body position and that for estimating the respiratory state separately. Thus, the sleep sensor **10** can be made small, light and thin in the present embodiment.

Further, in the present embodiment, since processing can be performed appropriately even by the A/D converter **106d** of low resolution as the alternating-current component extracted from the acceleration signal detected by the acceleration signal detector **111** is amplified, there is no need to use an expensive A/D converter **106d** and cost reduction can be realized.

Although it has been described that in the present embodiment, the respiratory signal detector **113** is operated when the user's body position is the supine position in terms of the fact that snoring is likely to occur in the supine position, a structure in which the respiratory signal detector **113** is operated in a predefined body position other than the supine position, for example, can also be adopted.

In addition, although it has been mainly described that the sleep sensor **10** is attached to the user's chest in the present embodiment, the sleep sensor **10** may be attached to other parts of the body as long as the user's body position and the respiratory state during sleep can be estimated by using the acceleration signal sensed by the acceleration sensor **106a**, for example.

Further, although it has been described that the sleep sensor **10** includes the body position estimation module **112** and the respiratory state estimation module **114** in the present embodiment, a structure in which processing executed by the body position estimation module **112** and the respiratory state estimation module **114** is executed by, for example, an external Bluetooth-enabled device or a server apparatus, etc. can also be adopted.

Furthermore, means for communicating with the outside may be a wireless communication system other than Bluetooth, and the sleep sensor **10** may be a structure capable of storing data in a memory installed inside the sleep sensor **10** and outputting data after completion of the measurement by means such as USB.

Second Embodiment

Next, a second embodiment will be described. The point that a microphone is used for estimating the user's respira-

tory state (presence or absence of a symptom of snoring) in the present embodiment is different from the first embodiment described above.

FIG. **6** is a diagram showing a system configuration of a sleep sensor **20** according to the present embodiment. In FIG. **6**, the same reference numbers are assigned to parts which are similar to those in FIG. **2** described above, and detailed explanation of them are omitted. Here, parts which are different from the configuration shown in FIG. **2** will be mainly described. Further, since usage of the sleep sensor **20** according to the present embodiment is as described with reference to FIG. **1** above, detailed explanation of the usage will be omitted.

As shown in FIG. **6**, the sleep sensor **20** further includes a microphone **201** in addition to the system configuration of the above-described first embodiment.

The microphone **201** is used for estimating a respiratory state of the user during sleep, and senses a sound signal generated in accordance with the user's respiratory state. With the use of the microphone **201**, a sound around the sleep sensor **20** can be converted into an electrical signal (a sound signal).

FIG. **7** is a block diagram showing mainly a functional configuration of the sleep sensor **20** according to the present embodiment. In FIG. **7**, the same reference numbers are assigned to parts which are the same as those in FIG. **4** described above, and detailed explanation of them are omitted. Here, parts which are different from the configuration shown in FIG. **4** will be mainly described.

As shown in FIG. **7**, the sleep sensor **20** includes a sound signal detector **211**, a respiratory state estimation module **212**, and a control module **213**, in addition to the acceleration signal detector **111** and the body position estimation module **112** of the first embodiment described above.

The sound signal detector **211** is a functional module which is realized by the microphone **201** described above, and detects the sound signal by using the microphone **201**. The sound signal detected by the sound signal detector **211** includes, for example, a signal of a respiratory sound, etc., which is generated by the user's symptom of snoring during sleep (hereinafter referred to as a snore signal), as the sound signal generated in accordance with the user's respiratory state.

The respiratory state estimation module **212** estimates the user's respiratory state during sleep based on the sound signal detected by the sound signal detector **211**. The user's respiratory state estimated by the respiratory state estimation module **212** includes, for example, presence or absence of a symptom of snoring during sleep.

The control module **213** controls the operation of the sound signal detector **211**. Specifically, the control module **213** executes the control to operate the sound signal detector **211** when the user's body position estimated by the body position estimation module **112** is a predefined body position (for example, the supine position).

The respiratory state estimation module **212** is a functional module which is realized when the above mentioned CPU **101** executes predetermined software (program). Further, the control module **213** is a functional module which is realized by, for example, a system controller **10**.

Next, referring to the flowchart of FIG. **8**, a processing procedure when the sleep sensor **20** according to the present embodiment estimates the user's sleep state the body position and the respiratory state) will be described.

First of all, processing of steps **S11** to **S13** corresponding to the processing of steps **S1** to **S3** shown in FIG. **5** described above is executed.

In step S13, when it is determined that the user's body position is the supine position (YES in step S13), the control module 213 executes the control of starting the operation of the sound signal detector 211 (step S14). In this case, the control module 213 powers on the sound signal detector 211 (that is, the microphone 201). Accordingly, the sound signal detector 211 is able to detect a sound signal.

In this case, by using the microphone 201, the sound signal detector 211 detects the sound signal representing a sound around the sleep sensor 20 (step S15).

Next, the respiratory state estimation module 212 estimates presence or absence of a symptom of snoring, for example, as the user's respiratory state during sleep, on the basis of the sound signal detected by the sound signal detector 211 (step S16). In this case, when the respiratory state estimation module 212 determines that the sound signal includes the aforementioned snore signal as a result of analyzing the sound signal detected by the sound signal detector 211, the respiratory state estimation module 212 can determine that the user shows the symptom of snoring.

Meanwhile, when it is determined that the user's body position is not the supine position so the above step S13 (NO in step S13), the control module 213 executes the control of stepping the operation of the sound signal detector 211 (step S17). In this case, the control module 213 powers off the sound signal detector 211 (that is the microphone 201). When this is carried out, since the sound signal, detector 211 cannot detect a sound signal, the processing of the sleep sensor 20 is terminated.

It should be noted that the result of estimation of the user's body position in the above step S12, and the result of estimation of the user's respiratory state in step S16 are transmitted to, for example, an external Bluetooth-enabled device or a server apparatus, etc., as in the first embodiment described above.

As described above, in the present embodiment, the control to operate the sound signal detector 211 is executed when the estimated user's body position is a predefined body position (for example, the supine position). In the present embodiment, by this structure, since the sound signal is detected (that is, the user's respiratory state is estimated) only when the user's body position is the supine position as in the first embodiment described above, it becomes possible to reduce the power consumption when the user's body position is not the supine position.

Note that in the present embodiment, since the acceleration signal is used for only estimating the user's body position and there is no need to extract an alternating-current component from the acceleration signal, a structure in which an acceleration sensor module 106 does not include a high-pass filter 106b and an amplifier circuit 106c may be adopted. Also, in the above first embodiment, it has been described that the acceleration sensor 106a outputs an analog signal. However, as long as the acceleration sensor 106a enables the user's body position to be estimated, the acceleration sensor 106a of the present embodiment may output a digital signal.

Further, although it has been described that the sound signal detector 211 is operated when the user's body position is the supine position in the present embodiment, a structure in which the sound signal detector 211 is operated in a predefined body position other than the supine position, for example, can also be adopted.

Furthermore, although it has been described that an attachment surface of the sleep sensor 20 is adhered to the user's chest in its use in the present embodiment, as long as the user's body position during sleep can be estimated by

using the acceleration signal sensed by the acceleration sensor 106a, for example, and the user's respiratory state during sleep can be estimated by using the sound signal sensed by the microphone 201, the sleep sensor 20 may be attached to other parts of the body.

Moreover, although it has been described that the sleep sensor 20 includes the body position estimation module 112 and the respiratory state estimation module 212 in the present embodiment, a structure in which processing executed by the body position estimation module 112 and the respiratory state estimation module 212 is executed by, for example, an external Bluetooth-enabled device or a server apparatus, etc. can also be adopted.

Third Embodiment

Next, a third embodiment will be described. In the present embodiment, the point that a microphone is used for estimating the user's respiratory state is the same as the second embodiment. However, the point that the microphone has directivity to a predetermined direction (high sound collecting capability) is different from the second embodiment described above. Since the system configuration of a sleep sensor according to the present embodiment is similar to that of the above-described second embodiment, explanation will be given by referring to FIG. 6 as necessary.

FIG. 9 is an illustration for describing the shape of a sleep sensor 30 according to the present embodiment. Note that the sleep sensor 30 according to the present embodiment is used by having an attachment surface of the sleep sensor 30 adhered to the user's chest, etc., as in the case of the first and second embodiments described above.

As shown in FIG. 9, in the present embodiment, the sleep sensor 30 includes a housing in the shape of stethoscope for example, and an acceleration sensor module 106 and a microphone 201 are arranged on the housing. Also, in this housing, a hole 31 is provided at a place where the microphone 201 is arranged in the direction of the attachment surface of the sleep sensor 30. In the present embodiment, because of such hole 31, the microphone 201 has directivity to the side of the attachment surface (that is, toward the interior of the user's body when the sleep sensor 30 is attached to the user). Further, as the microphone 201 of the present embodiment, a MEMS microphone or the like is used. Also, the microphone 201 (and the acceleration sensor module 106) is to be covered by a cover member or the like in order to reduce the influence of a sound, etc. around the sleep sensor 30, although this is not illustrated in FIG. 9. Further, instead of providing a hole as shown in FIG. 9, the microphone 201 may be mounted inside the mortar configuration.

FIG. 10 is a block diagram showing mainly a functional configuration of the sleep sensor 30 according to the present embodiment. In FIG. 10, the same reference numbers are assigned to parts which are the same as those in FIGS. 4 and 7 described above, and detailed explanation of them are omitted. Here, parts which are different from the configuration shown in FIGS. 4 and 7 will be mainly described.

As shown in FIG. 10, the sleep sensor 30 includes an intracorporeal sounds signal detector 311, a respiratory state estimation module 312, and a control module 313, in addition to the acceleration signal detector 111 and the body position estimation module 112 of the first and the second embodiments described above.

The intracorporeal sound signal detector 311 is a functional module which is realized by the microphone 201, and detects a sound signal, by using the microphone 201. Fur-

ther, since the microphone **201** of the present embodiment has directivity as described above, a sound signal detected by the intracorporeal sound signal detector **311** is an intracorporeal sound signal representing the user's intracorporeal sound.

The respiratory state estimation module **312** estimates the user's respiratory state during sleep based on the intracorporeal sound signal detected by the intracorporeal sound signal detector **311**. The user's respiratory state estimated by the respiratory state estimation module **312** includes, for example, presence or absence of a symptom of snoring during sleep.

The control module **313** controls the operation of the sound signal detector **311**. Specifically, the control module **313** executes the control to operate the intracorporeal sound signal detector **311** when the direction of gravitational acceleration calculated from an acceleration signal detected by the acceleration signal detector **111** agrees with the directivity of the microphone **201**.

Note that the respiratory state estimation module **312** is a functional module which is realized when the above-mentioned CPU **101** executes predetermined software (program). Further, the control module **313** is a functional module which is realized by, for example, a system controller **105**.

Next, referring to the flowchart of FIG. **11**, a processing procedure when the sleep sensor **30** according to the present embodiment estimates the user's sleep state (the body position and the respiratory state) will be described.

First of all, processing of steps **S21** and **S22** corresponding to the processing of steps **S1** and **S2** shown in FIG. **5** described above is executed.

Next, it is determined whether the direction of gravitational acceleration in the user's body position estimated in step **S22** agrees with the orientation of directivity of the microphone **201** (step **S23**).

When it is determined that the direction of gravitational acceleration agrees with the orientation of directivity of the microphone **201** (YES in step **S23**), the control module **313** executes the control of starting the operation of the intracorporeal sound signal detector **311** (step **S24**). In this case, the control module **313** powers on the intracorporeal sound signal detector **311** (that is, the microphone **201**). Accordingly, the intracorporeal sound signal, detector **311** is able to detect an intracorporeal sound signal.

In this case, by using the microphone **201**, the intracorporeal sound signal detector **311** detects the intracorporeal sound signal representing the user's intracorporeal sound (step **S25**).

Next, the respiratory state estimation module **312** estimates presence or absence of a symptom of snoring, for example, as the user's respiratory state during sleep, on the basis of the intracorporeal sound signal detected by the intracorporeal sound signal detector **311** (step **S26**). In this case, an intracorporeal sound signal, etc., when snoring occurs, for example, is stored in the sleep sensor **30** in advance, and by comparing the stored intracorporeal sound signal with the intracorporeal sound signal detected by the intracorporeal sound signal detector **311**, whether or not the user shows a symptom of snoring can be estimated.

Meanwhile, when it is determined that the direction of gravitational acceleration does not agree with the orientation of directivity of the microphone **201** in step **S23** (NO in step **S23**), the control module **313** executes the control of stopping the operation of the intracorporeal sound signal detector **311** (step **S27**). In this case, the control module **313** powers off the intracorporeal sound signal detector **311** (that

is, the microphone **201**). When this is carried out, since the intracorporeal sound signal detector **311** cannot detect an intracorporeal sound signal, the processing of the sleep sensor **30** is terminated.

It should be noted that the result of estimation of the user's body position in the above step **S22**, and the result of estimation of the user's respiratory state in step **S25** are transmitted to, for example, an external Bluetooth-enabled device or a server apparatus, etc., as in the first and the second embodiments described above.

As described above, in the present embodiment, when the direction of gravitational acceleration that acts on the sleep sensor **30** agrees with the orientation of directivity of the microphone **201**, the control to operate the intracorporeal sound signal detector **311** is executed.

Here, in order to accurately detect an intracorporeal sound signal, it is important that the microphone **201** be brought into close contact with the user's body surface. Therefore, in the present embodiment, an intracorporeal sound signal is detected (i.e., the user's respiratory state is estimated) only when the direction of gravitational acceleration that acts on the sleep sensor **30** agrees with the directivity of the microphone **201** (that is, the direction toward the interior of the user's body), in other words, the sleep sensor **30** is closely adhered to the user's body surface by its own weight. In this way, it is possible to accurately detect an intracorporeal sound signal, and also reduce the power consumption in a case where the sleep sensor **30** is not closely adhered to the body surface and the intracorporeal sound cannot be detected accurately.

Also, since the user's intracorporeal sound signal in the present embodiment is hard to be subjected to the influence of disturbance as compared to a sound signal around the sleep sensor **20** of the second embodiment described above, it becomes possible to more accurately estimate the user's respiratory state.

In the present embodiment, it has been described that the control to detect an intracorporeal sound signal is executed when the direction of gravitational acceleration that acts on the sleep sensor **30** agrees with the directivity of the microphone **201**. However, a structure of executing the control, to detect an intracorporeal sound signal when the user's body position is the supine position may also be adopted, as described in the above, first and second embodiments.

Further, when the sleep sensor **30** is attached to the user's chest as described above, the user's body position when the direction of gravitational acceleration that acts on the sleep sensor **30** agrees with the directivity of the microphone **201** is often the supine position (face-up posture). Accordingly, also in the present embodiment, an intracorporeal sound signal is detected when the user's body position is the supine position (that is, a body position in which snoring is likely to occur) as a consequence.

Also, since there is no need to extract an alternating-current component from an acceleration signal in the present embodiment, as in the second embodiment described above, a structure in which an acceleration sensor module **106** does not include, a high-pass filter **106b** and an amplifier circuit **106c** may be adopted. Further, an acceleration sensor **106a** of the present embodiment may be one which outputs an analog signal or one which outputs a digital signal as in the second embodiment described above.

In addition, although it has been described that an attachment surface of the sleep sensor **30** is adhered to the user's chest in its use in the present embodiment, as long as, for example, the user's body position during sleep can be estimated by using the acceleration signal sensed by the

13

acceleration sensor **106a** and the user's respiratory state during sleep can be estimated by using the intracorporeal sound signal sensed by the microphone **201**, the sleep sensor **30** may be attached to other parts of the body.

Further, although it has been described that the sleep sensor **30** includes the body position estimation module **112** and the respiratory state estimation module **312** in the present embodiment, a structure in which processing executed by the body position estimation module **112** and the respiratory state estimation module **312** is executed by for example, an external Bluetooth-enabled device or a server apparatus, etc. can also be adopted.

Furthermore, in each of the above-described embodiments, it has been described that the user's respiratory state as the state other than the user's body position is estimated. However, as long as the operation of the other sensor, etc. is controlled in accordance with the result of estimation of the user's body position, the present embodiment may be applied to a case of estimating a state other than the user's respiratory state.

According to at least one of the embodiments described above, a sleep sensor capable of achieving power-saving can be provided.

While certain embodiments have been described, these embodiments have been presented by way of example only, and are not intended to limit the scope of the inventions. Indeed, these embodiments may be embodied in a variety of other forms; furthermore, various omissions, substitutions and changes in the form of the embodiment described herein may be made without departing from the spirit of the invention. The accompanying claims and their equivalents are intended to cover such forms or modifications as would fall within the scope and spirit of the inventions.

14

What is claimed is:

1. A sleep sensor which is attachable to a user who is sleeping when it is to be used, the sleep sensor detecting snoring for monitoring a respiratory state of the user and comprising:

a first sensor configured to detect an acceleration signal representing acceleration that acts on the sleep sensor; a second sensor configured to detect a signal for estimating the state of the user; and

a processor configured to:

estimate the user's body position based on the detected acceleration signal, and

operate the second sensor when the estimated user's body position is at least one of predefined body positions, wherein:

the acceleration signal detected by the first sensor includes a direct-current component representing gravitational acceleration that acts on the sleep sensor,

the second sensor includes a microphone having directivity to a side of an attachment surface of the sleep sensor and configured to detect an intracorporeal sound signal which is generated in accordance with the user's respiratory state as a signal for estimating the user's respiratory state, and

the processor is further configured to:

determine whether a direction of the gravitational acceleration agrees with the directivity of the microphone in the estimated user's body position,

power on the microphone when the direction of the gravitational acceleration agrees with the directivity of the microphone in the estimated user's body position, and

power off the microphone when the direction of the gravitational acceleration does not agree with the directivity of the microphone.

* * * * *

专利名称(译)	睡眠传感器		
公开(公告)号	US10045733	公开(公告)日	2018-08-14
申请号	US14/749106	申请日	2015-06-24
[标]申请(专利权)人(译)	株式会社东芝		
申请(专利权)人(译)	株式会社东芝		
当前申请(专利权)人(译)	TDK株式会社		
[标]发明人	TAKAKURA JUNYA NAKAYAMA KANAKO YAMAUCHI YASUNOBU		
发明人	TAKAKURA, JUNYA NAKAYAMA, KANAKO YAMAUCHI, YASUNOBU		
IPC分类号	A61B5/08 A61B5/00 A61B5/11 A61B7/00		
CPC分类号	A61B5/4818 A61B5/0826 A61B5/1116 A61B5/6823 A61B5/7285 A61B7/003 A61B5/7278 A61B2562/0219 A61B2560/0412 A61B2562/0204		
优先权	2014130290 2014-06-25 JP		
其他公开文献	US20150374284A1		
外部链接	Espacenet		

摘要(译)

根据一个实施例，提供了一种睡眠传感器，其连接到在使用时正在睡觉的用户。睡眠传感器包括第一检测器，估计模块，第二检测器和控制模块。第一检测器被配置为检测表示从睡眠传感器获得的加速度的加速度信号。估计模块被配置为基于检测到的加速度信号估计用户的身体位置。第二检测器被配置为检测用于估计除用户的身体位置之外的状态的信号。控制模块被配置为当估计的用户的身體位置是预定义的身体位置中的至少一个时操作第二检测器。

