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(54) **OPTICAL PATIENT MONITOR**

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A61B 5/1455	(2006.01)
A61B 5/0205	(2006.01)
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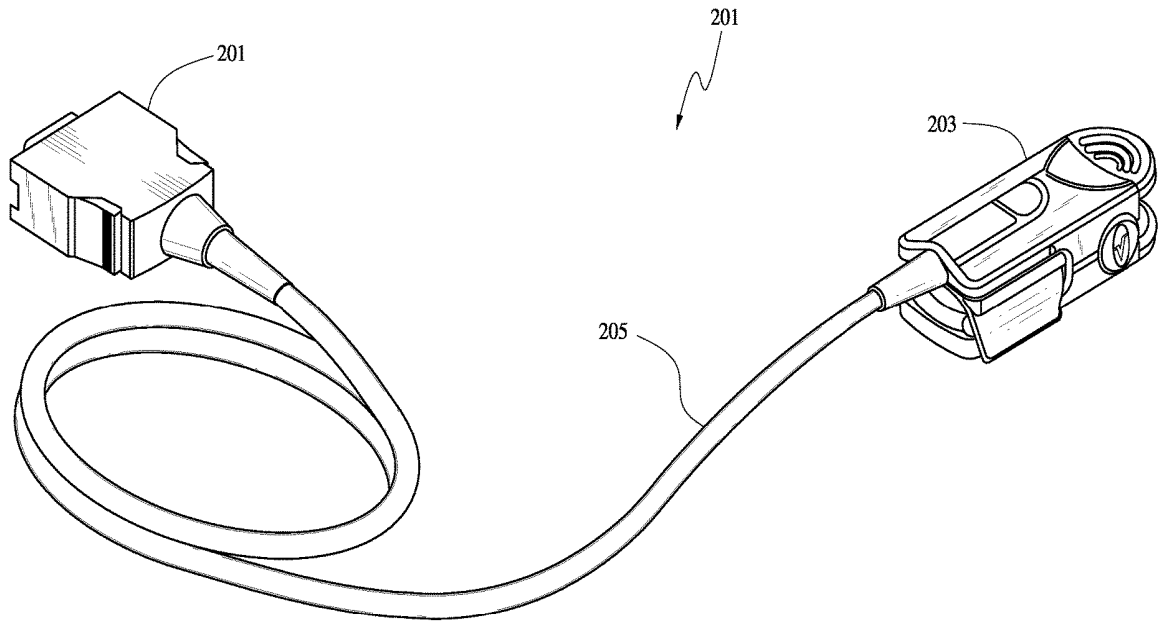
A61B 5/024	(2006.01)
A61B 5/0402	(2006.01)
A61B 5/145	(2006.01)

(52) **U.S. Cl.**

CPC ***A61B 5/7282*** (2013.01); *A61B 2562/222* (2013.01); ***G16H 40/63*** (2018.01); ***A61B 5/746*** (2013.01); ***A61B 5/08*** (2013.01); ***A61B 5/14551*** (2013.01); ***A61B 5/412*** (2013.01); ***A61B 5/6826*** (2013.01); ***A61B 5/6838*** (2013.01); ***A61B 5/7221*** (2013.01); ***A61B 5/0205*** (2013.01); ***A61B 5/7275*** (2013.01); ***A61B 5/01*** (2013.01); ***A61B 5/021*** (2013.01); ***A61B 5/024*** (2013.01); ***A61B 5/0402*** (2013.01); ***A61B 5/0816*** (2013.01); ***A61B 5/14532*** (2013.01); ***A61B 5/14539*** (2013.01); ***A61B 5/14546*** (2013.01); ***A61B 5/0004*** (2013.01); ***A61B 5/1455*** (2013.01); ***A61B 5/4839*** (2013.01); ***A61B 5/6832*** (2013.01); ***A61B 5/6843*** (2013.01); ***A61B 5/7246*** (2013.01); ***A61B 5/7405*** (2013.01); ***A61B 5/742*** (2013.01); *A61B 5/082* (2013.01); *A61B 5/14552* (2013.01); *A61B 2560/0285* (2013.01); *A61B 2560/0443* (2013.01); ***G16H 50/30*** (2018.01)

(57) **ABSTRACT**

An optical based patient monitoring system employing an optical sensor and providing an indication of an optical change which does not correlate to a change in a physiological blood parameter and based on that indication, providing a care provider an indication of a condition of a patient. The optical based patient monitoring system providing the indication of the patient condition in relation to a patient using an IV setup.



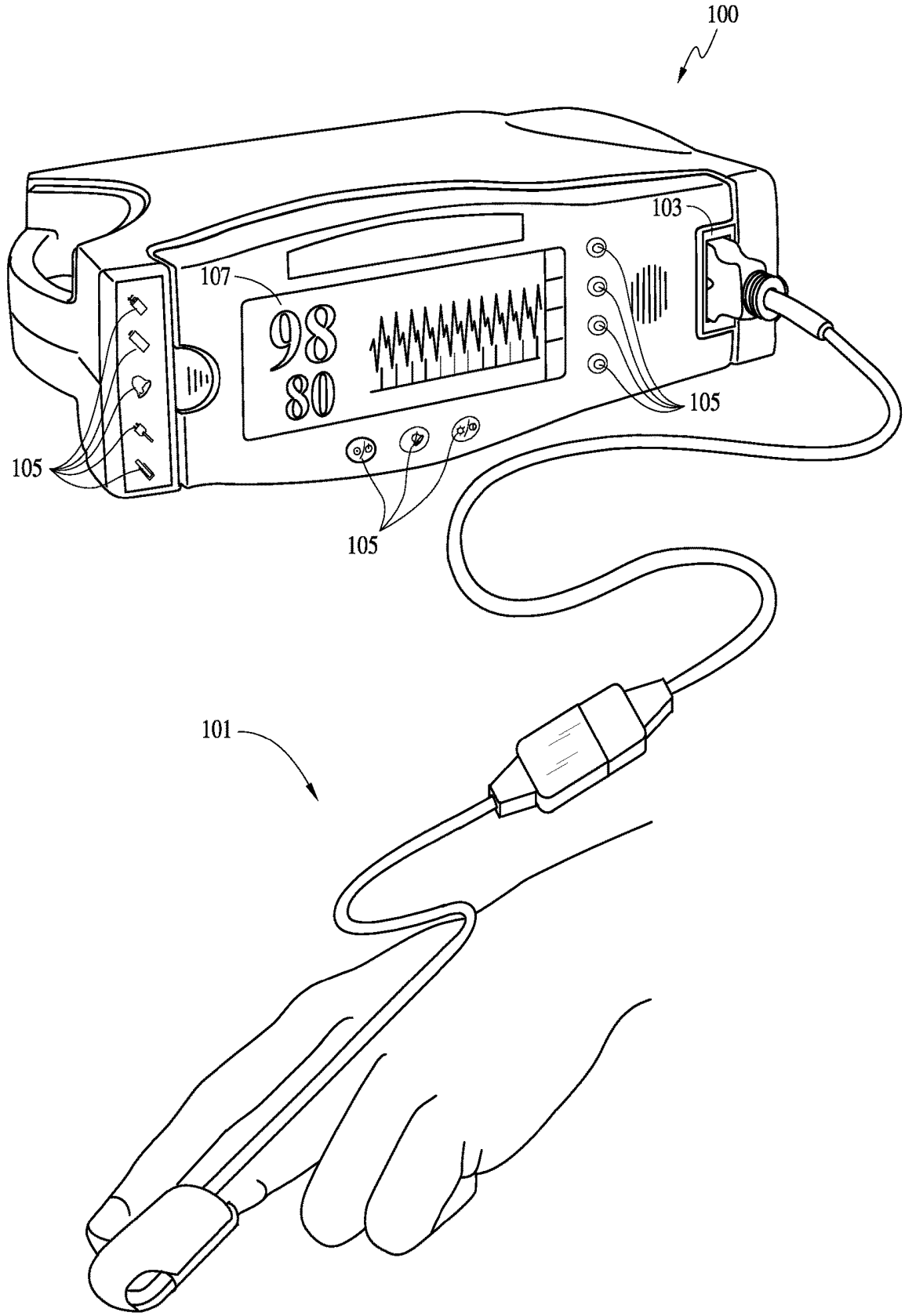


FIG. 1
(PRIOR ART)

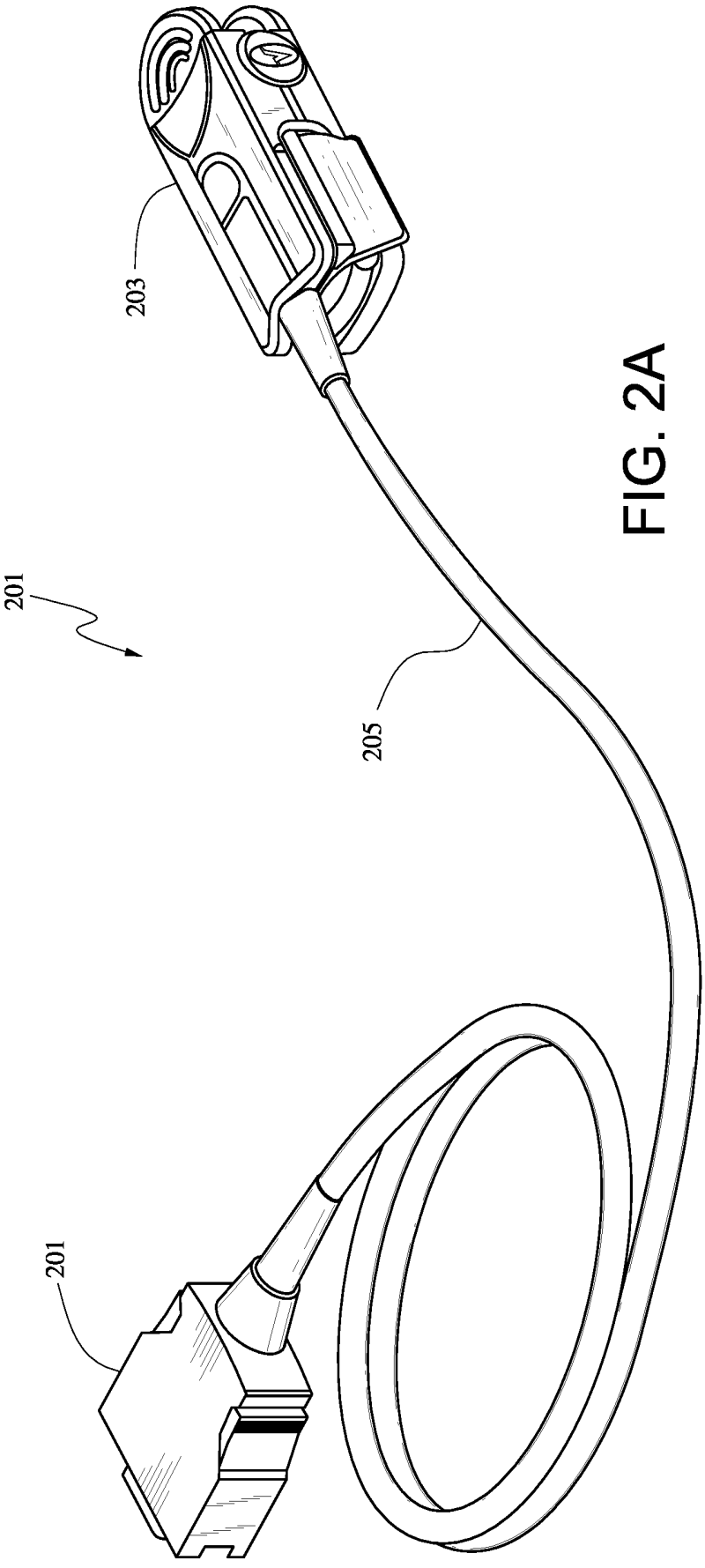


FIG. 2A

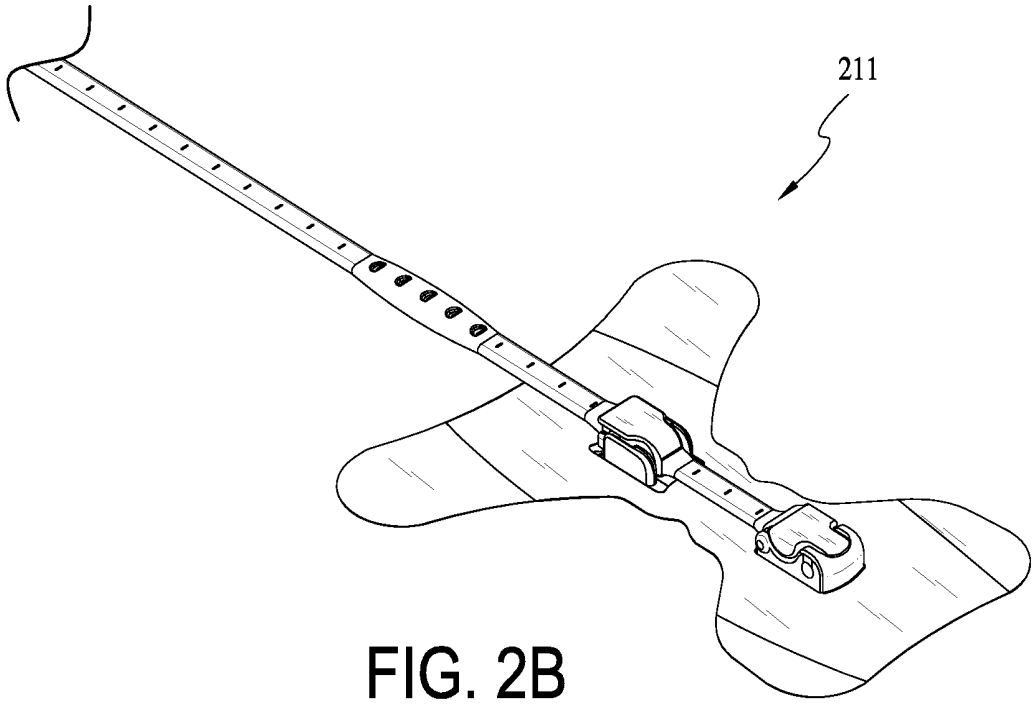


FIG. 2B

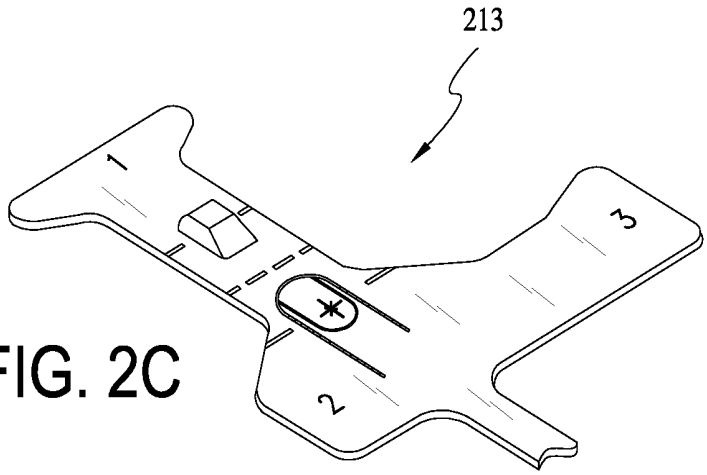


FIG. 2C

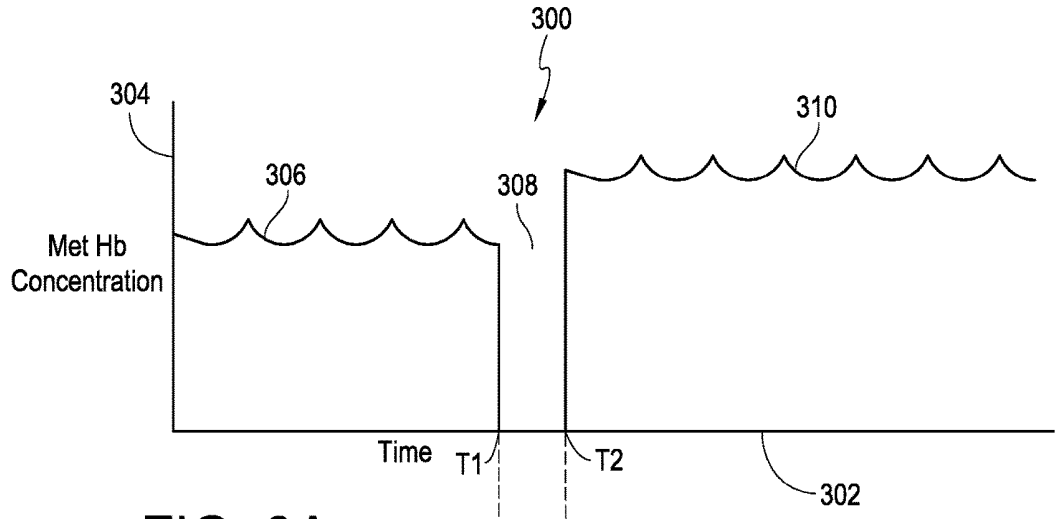

300
304
310
306
308
Met Hb
Concentration
Time
T1
T2
302

FIG. 3A

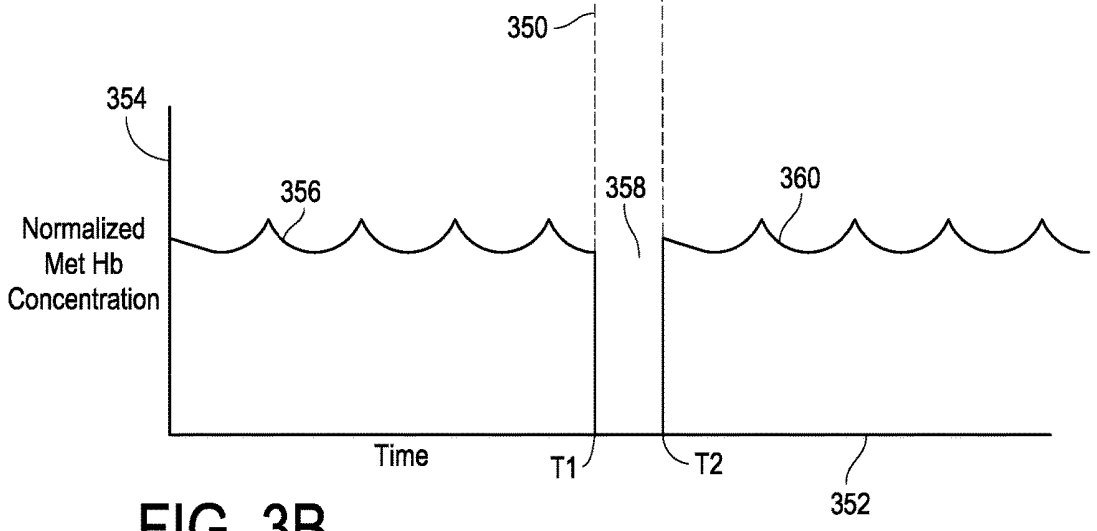

350
354
356
358
360
Normalized
Met Hb
Concentration
Time
T1
T2
352

FIG. 3B

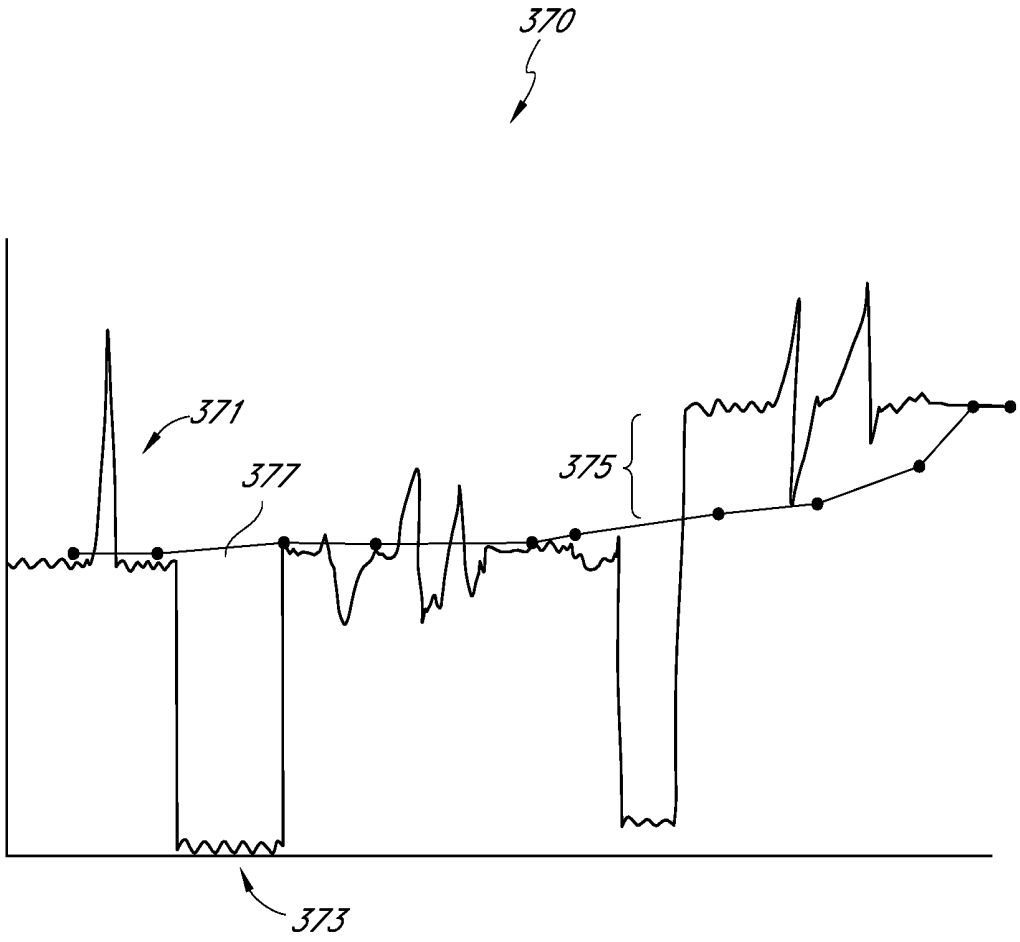


FIG. 3C

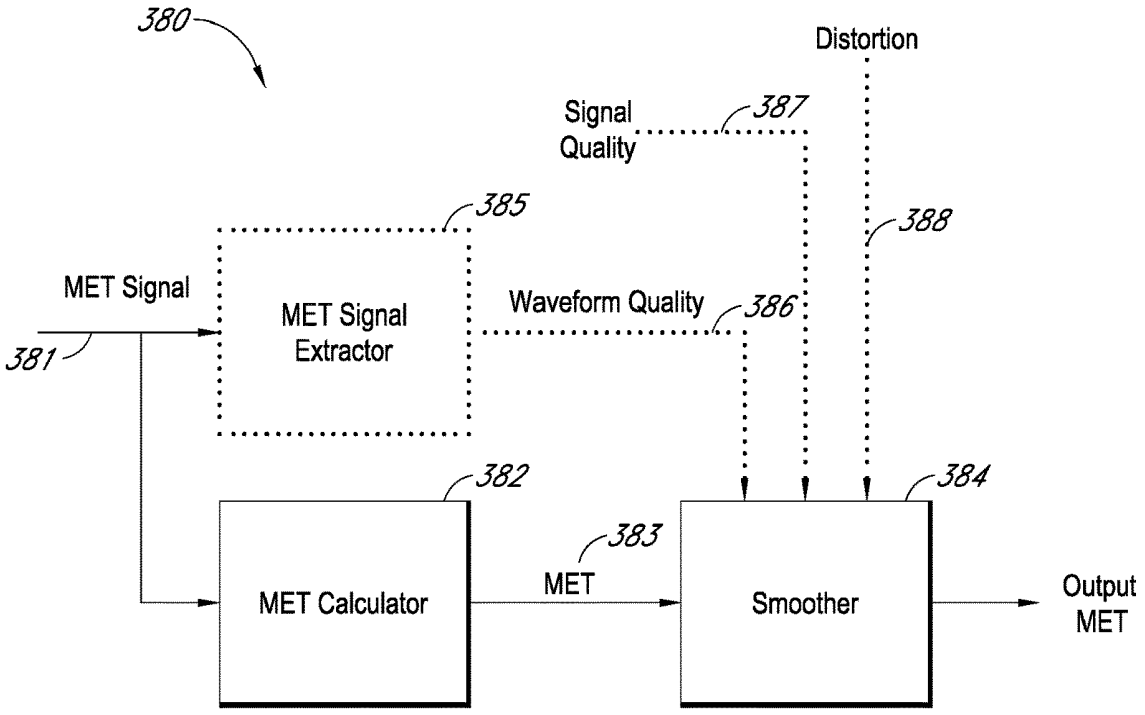

380
Distortion
Signal Quality
387
385
388
MET Signal
MET Signal Extractor
Waveform Quality
386
381
382
384
383
MET Calculator
MET
Smoother
Output MET

FIG. 3D

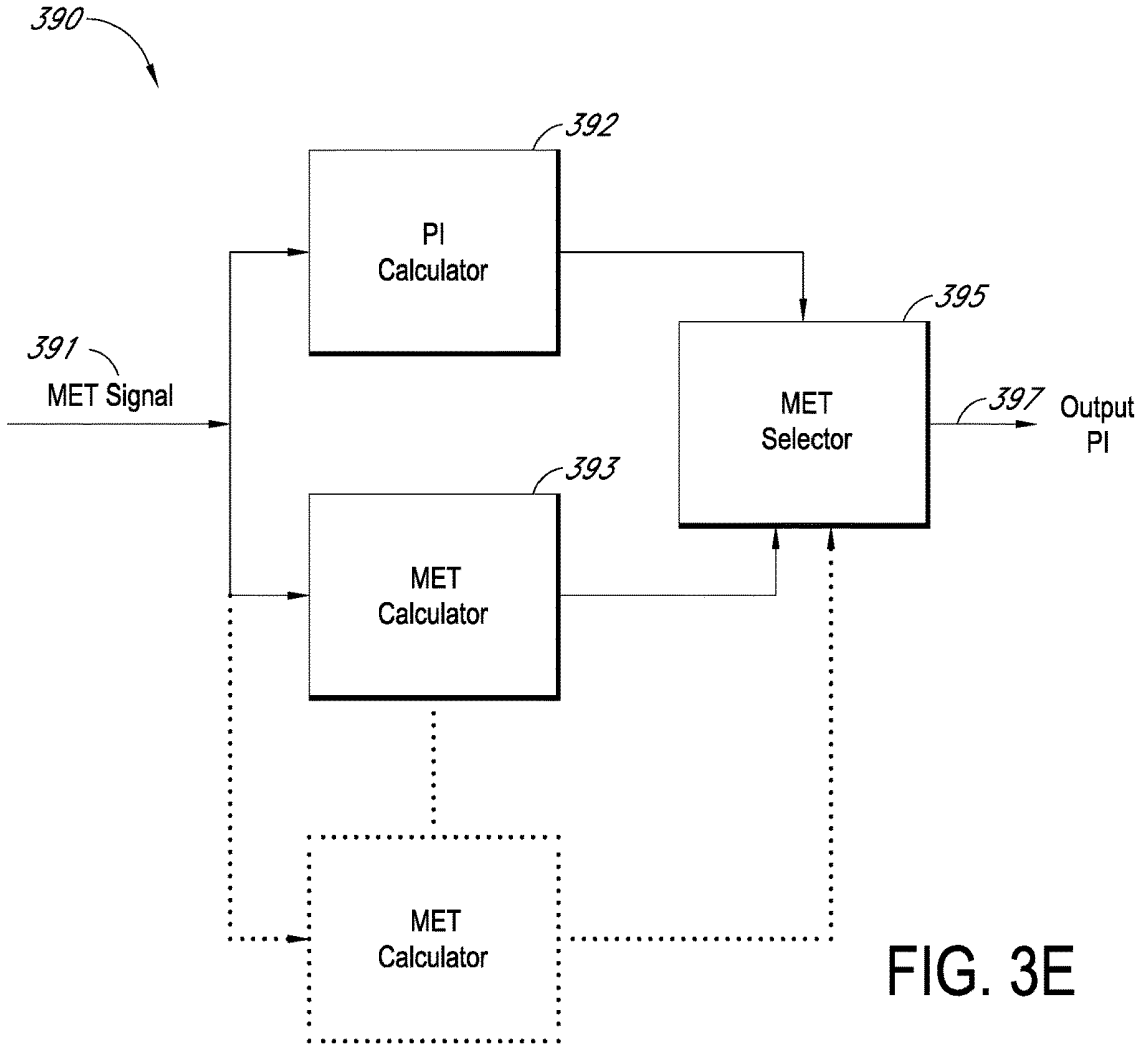

390
392
PI Calculator
395
391
MET Signal
MET Selector
397
Output PI
393
MET Calculator
MET Calculator

FIG. 3E

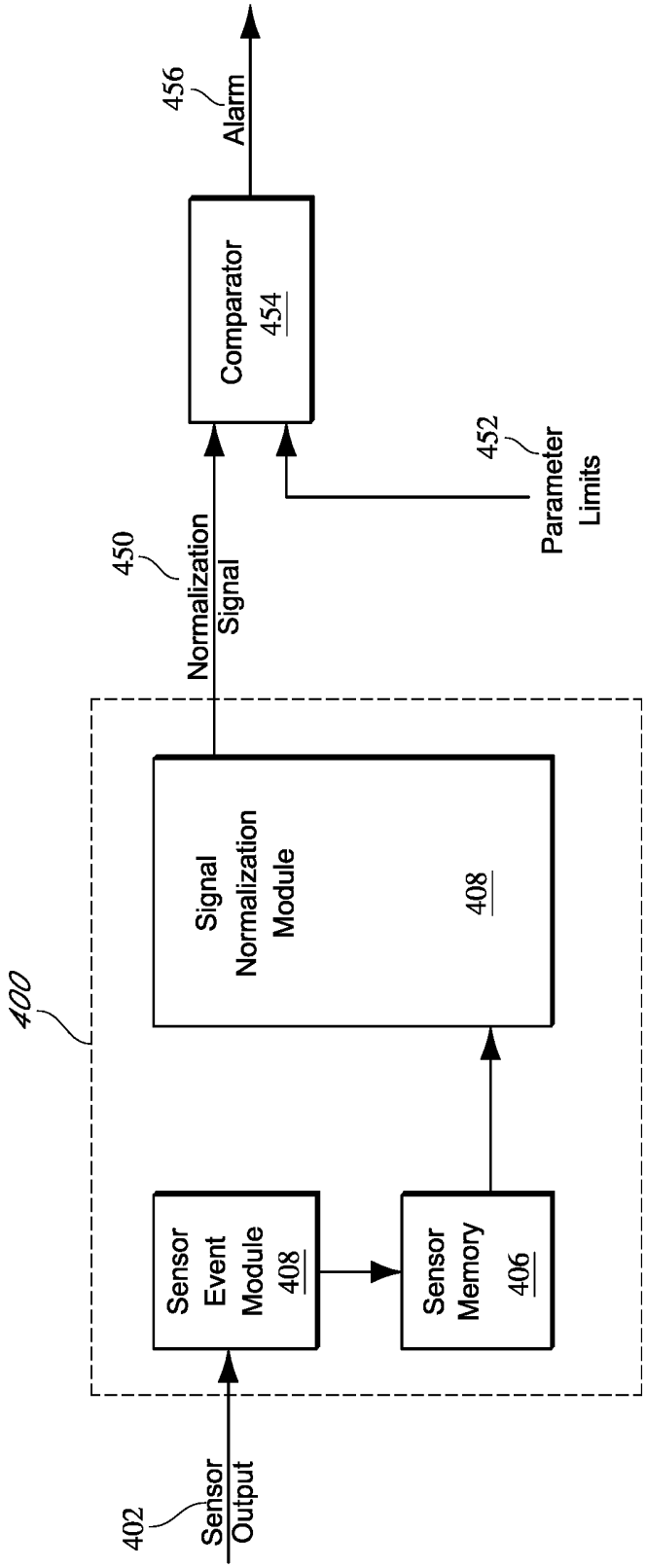

400
Sensor Output
402
Sensor Event Module 408
Sensor Memory 406
Signal Normalization Module 408
Normalization Signal
450
Parameter Limits
452
Comparator 454
Alarm
456

FIG. 4

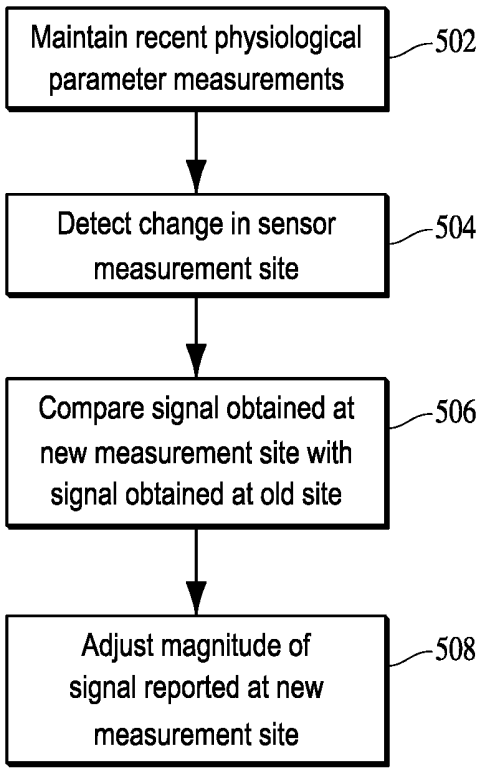

Maintain recent physiological parameter measurements
502
Detect change in sensor measurement site
504
Compare signal obtained at new measurement site with signal obtained at old site
506
Adjust magnitude of signal reported at new measurement site
508

FIG. 5

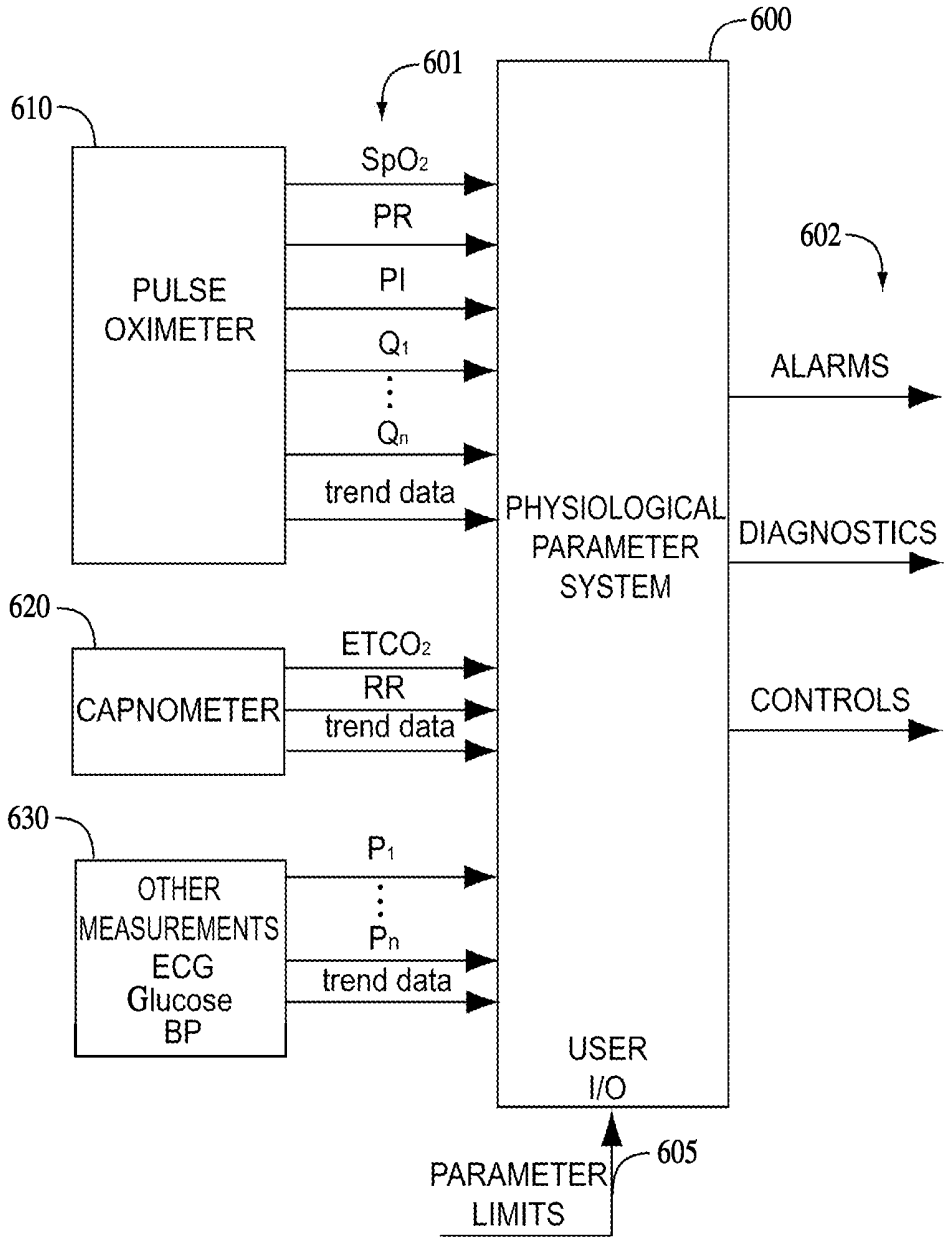

600
601
610
PULSE OXIMETER
SpO2
PR
PI
Q1
Qn
trend data
602
ALARMS
PHYSIOLOGICAL PARAMETER SYSTEM
DIAGNOSTICS
620
CAPNOMETER
ETCO2
RR
trend data
CONTROLS
630
OTHER MEASUREMENTS ECG Glucose BP
P1
Pn
trend data
USER I/O
PARAMETER LIMITS
605

FIG. 6

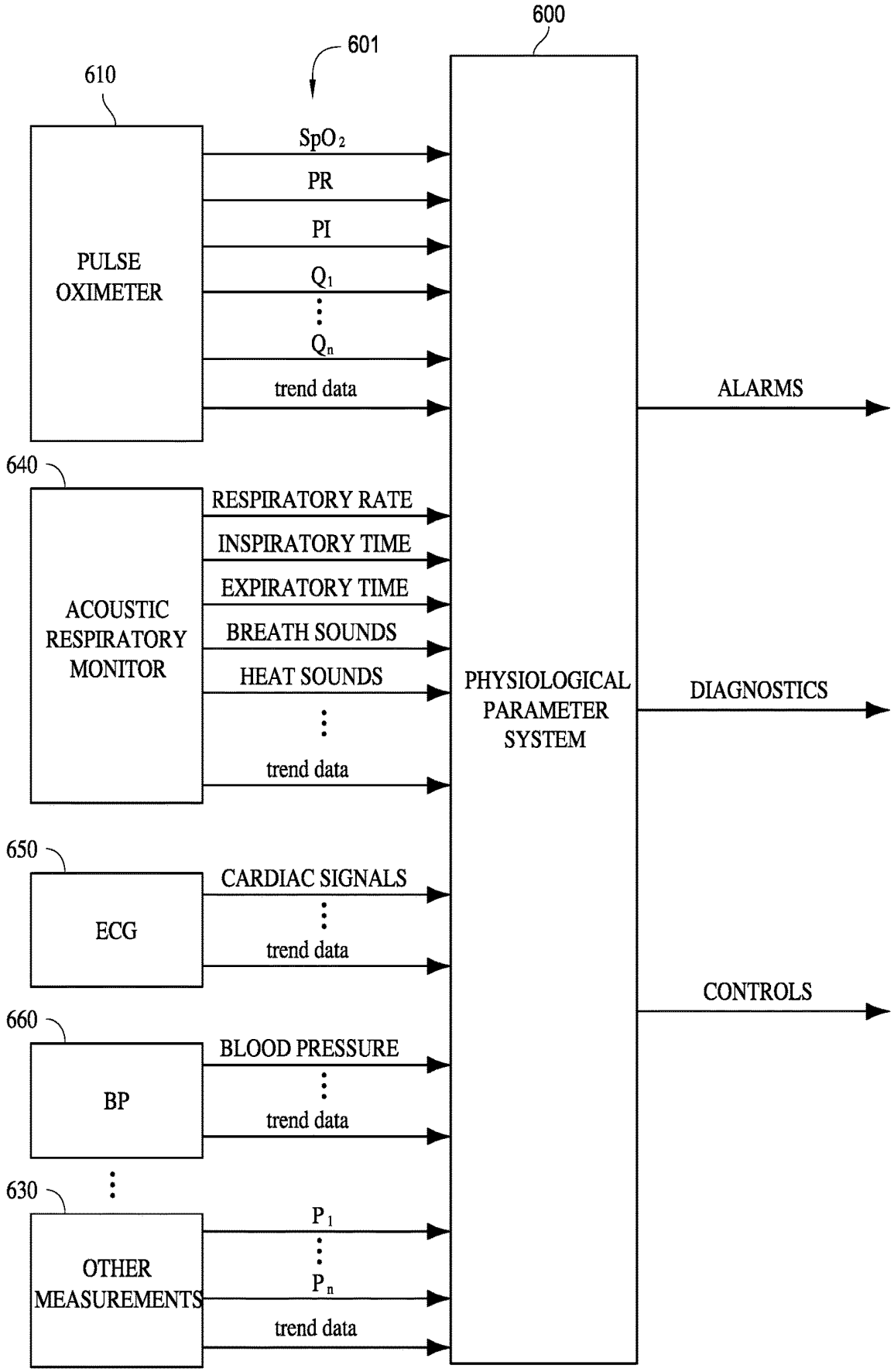

600
601
610
PULSE OXIMETER
SpO2
PR
PI
Q1
Qn
trend data
ALARMS
640
ACOUSTIC RESPIRATORY MONITOR
RESPIRATORY RATE
INSPIRATORY TIME
EXPIRATORY TIME
BREATH SOUNDS
HEAT SOUNDS
trend data
PHYSIOLOGICAL PARAMETER SYSTEM
DIAGNOSTICS
650
ECG
CARDIAC SIGNALS
trend data
CONTROLS
660
BP
BLOOD PRESSURE
trend data
630
OTHER MEASUREMENTS
P1
Pn
trend data

FIG. 6A

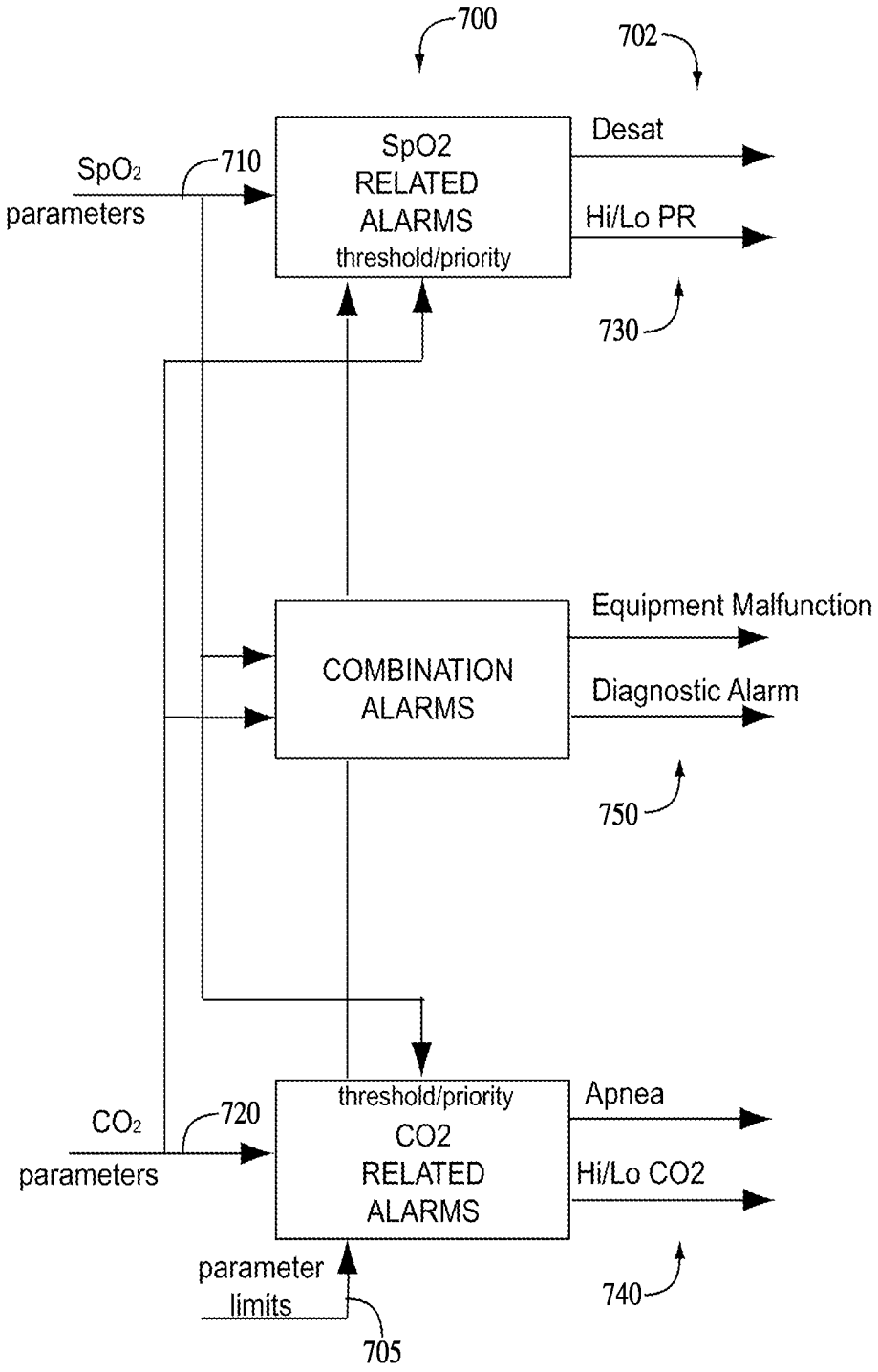

700
702
SpO2
RELATED
ALARMS
threshold/priority
Desat
Hi/Lo PR
730
SpO2
parameters
710
COMBINATION
ALARMS
Equipment Malfunction
Diagnostic Alarm
750
threshold/priority
CO2
RELATED
ALARMS
Apnea
Hi/Lo CO2
740
CO2
parameters
720
parameter
limits
705

FIG. 7

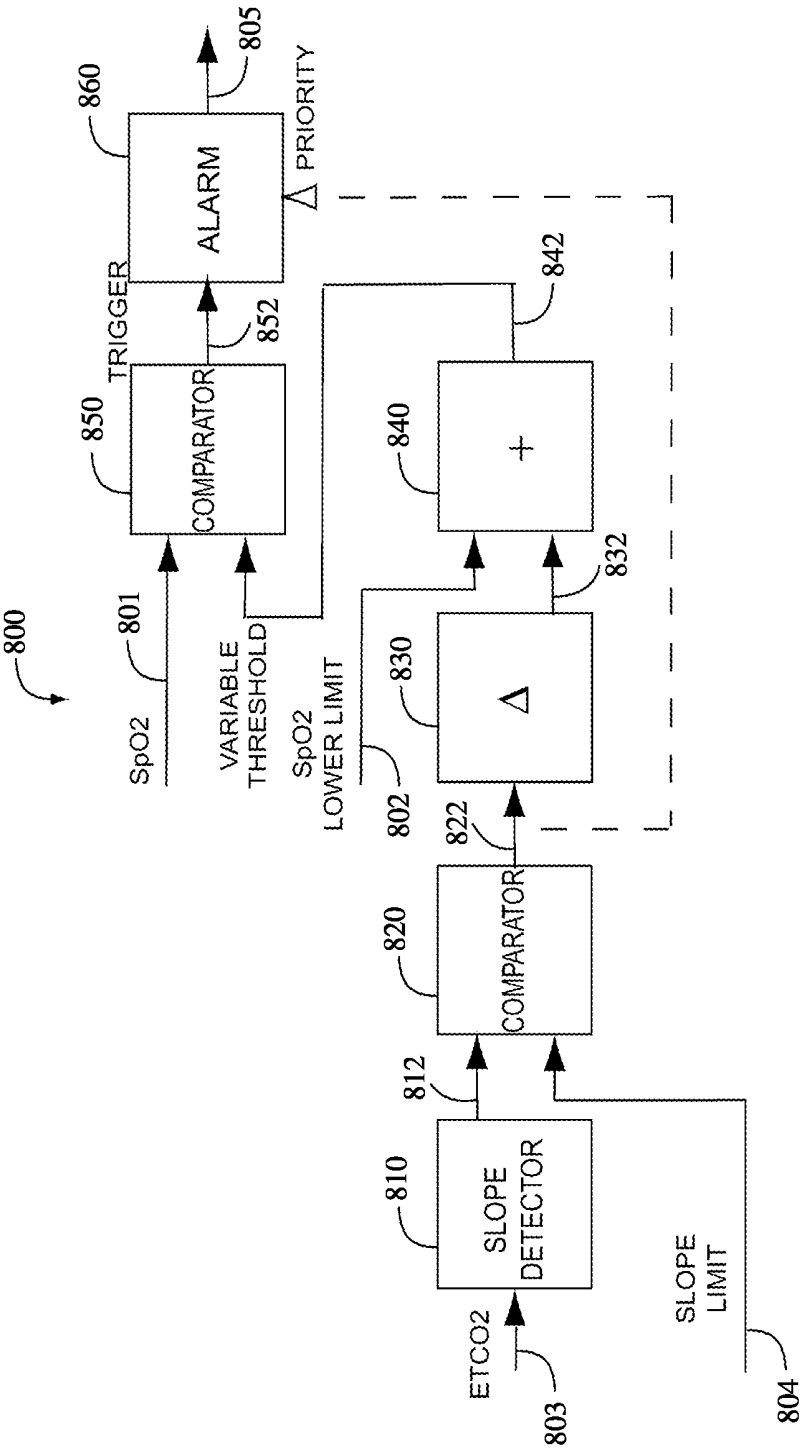

800
801
SpO2
VARIABLE THRESHOLD
SpO2 LOWER LIMIT
802
803
ETCO2
804
SLOPE LIMIT
805
810
SLOPE DETECTOR
812
820
COMPARATOR
822
830
Δ
832
840
+
842
850
COMPARATOR
852
TRIGGER
860
ALARM
PRIORITY

FIG. 8

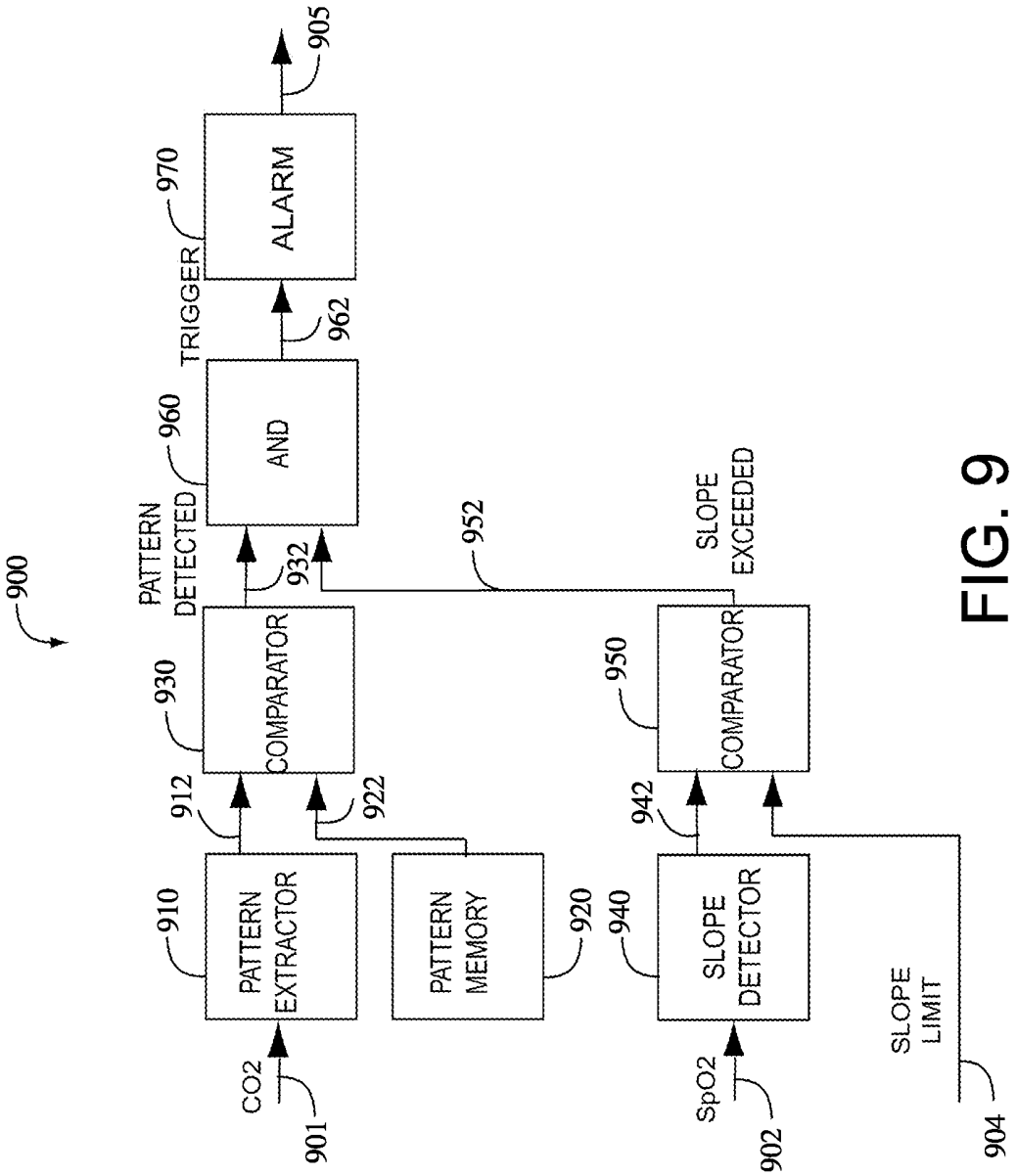

900
CO2
901
PATTERN EXTRACTOR
910
912
PATTERN MEMORY
920
922
COMPARATOR
930
PATTERN DETECTED
932
SpO2
902
SLOPE DETECTOR
940
942
COMPARATOR
950
SLOPE EXCEEDED
952
SLOPE LIMIT
904
AND
960
TRIGGER
962
ALARM
970
905

FIG. 9

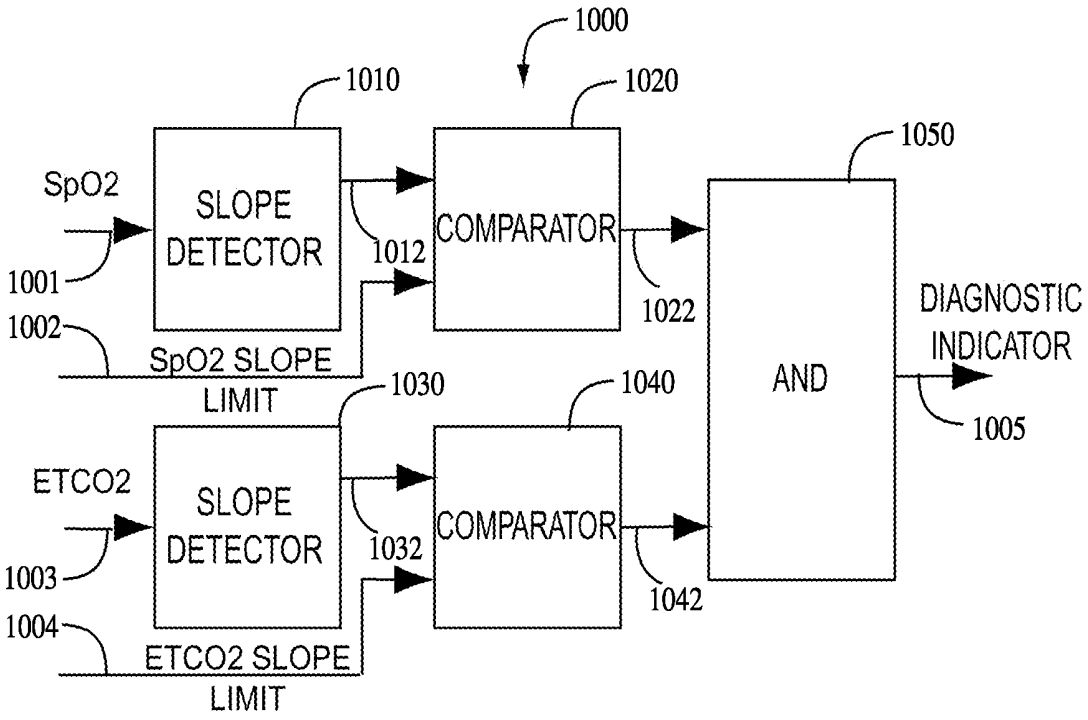

1000
1010
1020
1050
SpO2
SLOPE DETECTOR
COMPARATOR
1001
1012
1022
1002
SpO2 SLOPE LIMIT
AND
DIAGNOSTIC INDICATOR
1030
1040
1005
ETCO2
SLOPE DETECTOR
COMPARATOR
1003
1032
1042
1004
ETCO2 SLOPE LIMIT

FIG. 10

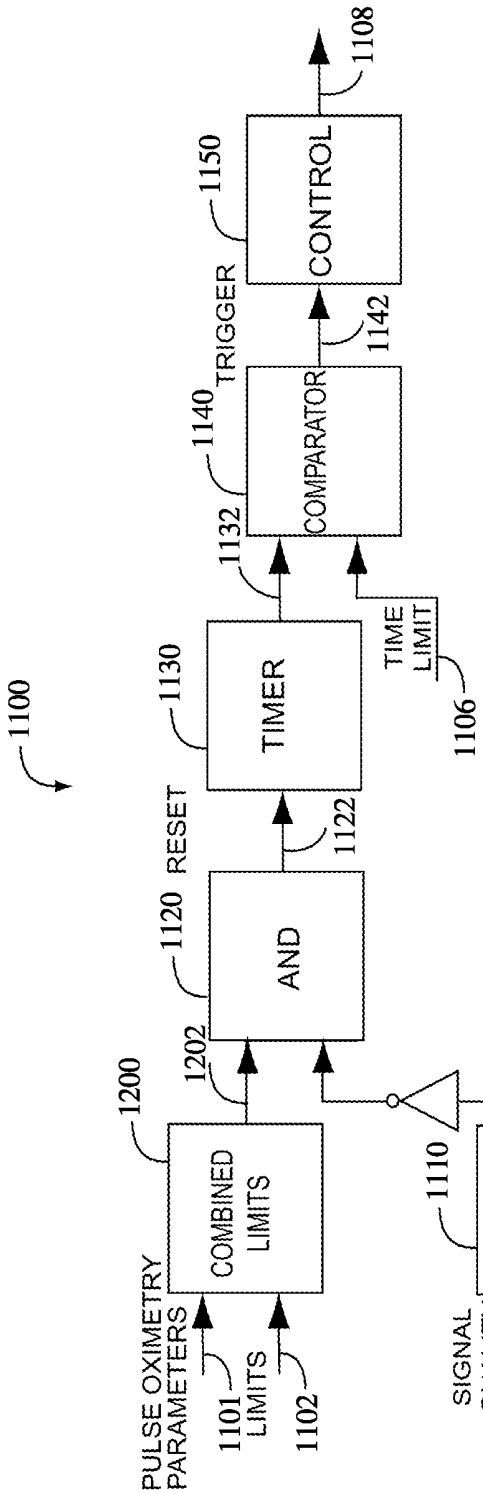

1100
PULSE OXIMETRY PARAMETERS
1101
LIMITS
1102
1200
COMBINED LIMITS
1202
SIGNAL QUALITY
1103
LOWER LIMIT
1104
1110
COMPARATOR
1112
1120
AND
RESET
1122
1130
TIMER
TIME LIMIT
1106
1132
1140
COMPARATOR
TRIGGER
1142
1150
CONTROL
1108

FIG. 11A

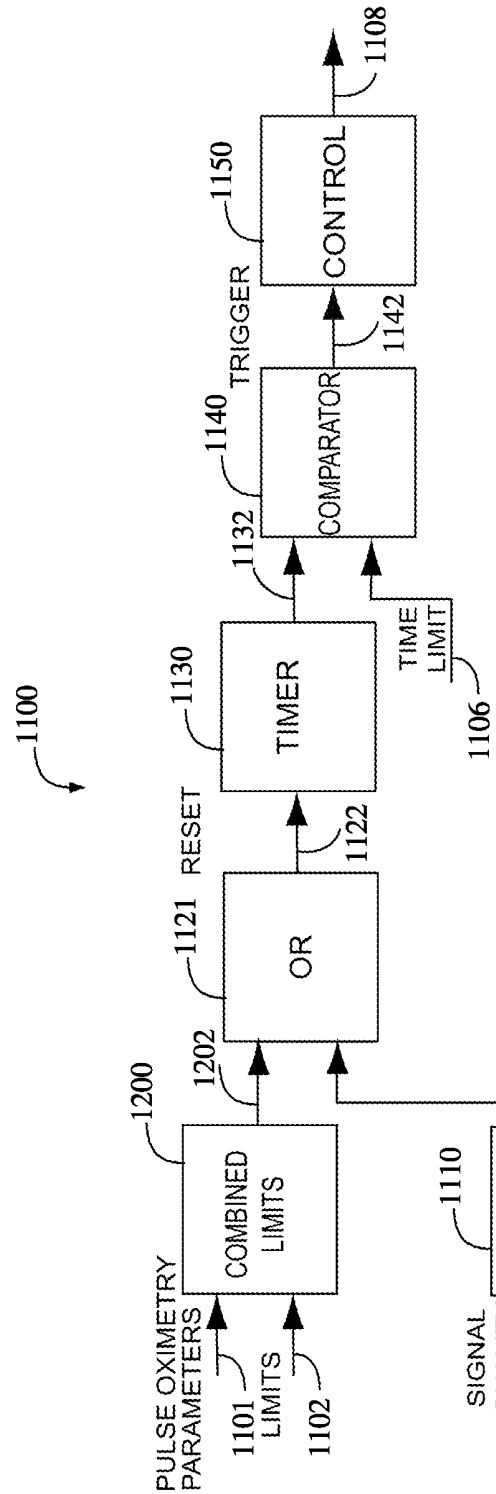

1100
PULSE OXIMETRY PARAMETERS
1101 LIMITS
1102
COMBINED LIMITS
1200
1202
SIGNAL QUALITY
1103
LOWER LIMIT
1104
COMPARATOR
1110
1112
OR
1121
RESET
1122
TIMER
1130
TIME LIMIT
1106
1132
COMPARATOR
1140
TRIGGER
1142
CONTROL
1150
1108

FIG. 11B

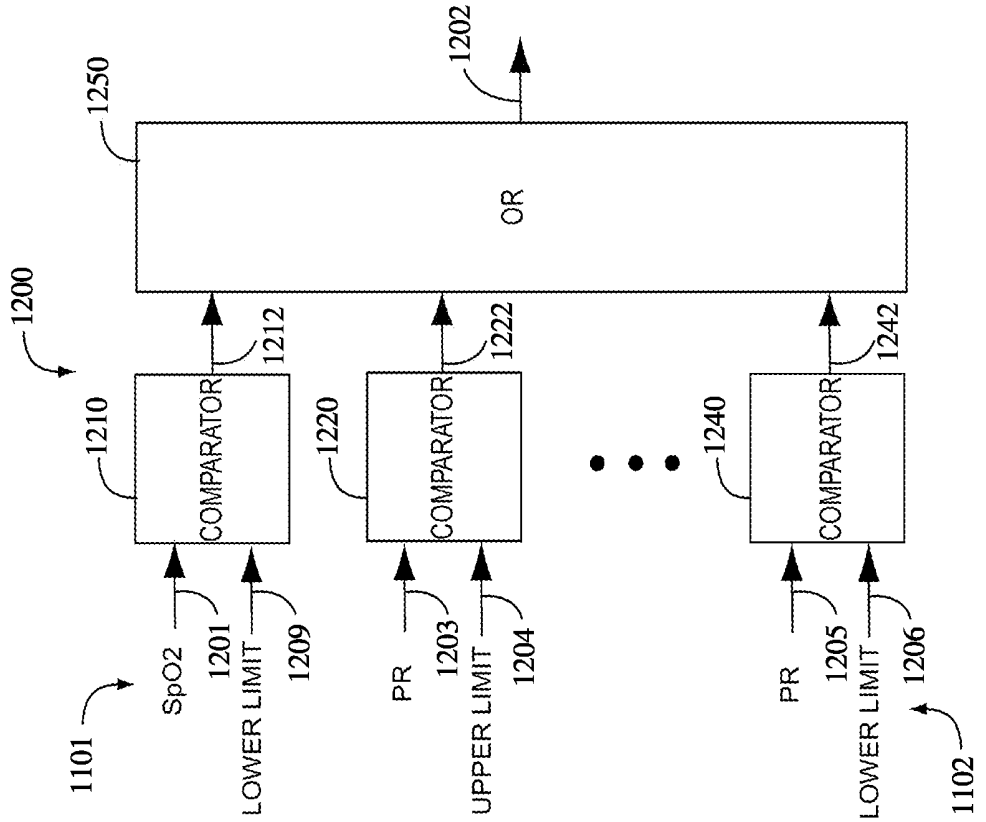

1200
1250
1202
OR
1210
COMPARATOR
1212
1220
COMPARATOR
1222
1240
COMPARATOR
1242
1101
SpO2
1201
LOWER LIMIT
1209
PR
1203
UPPER LIMIT
1204
PR
1205
LOWER LIMIT
1206
1102

FIG. 12

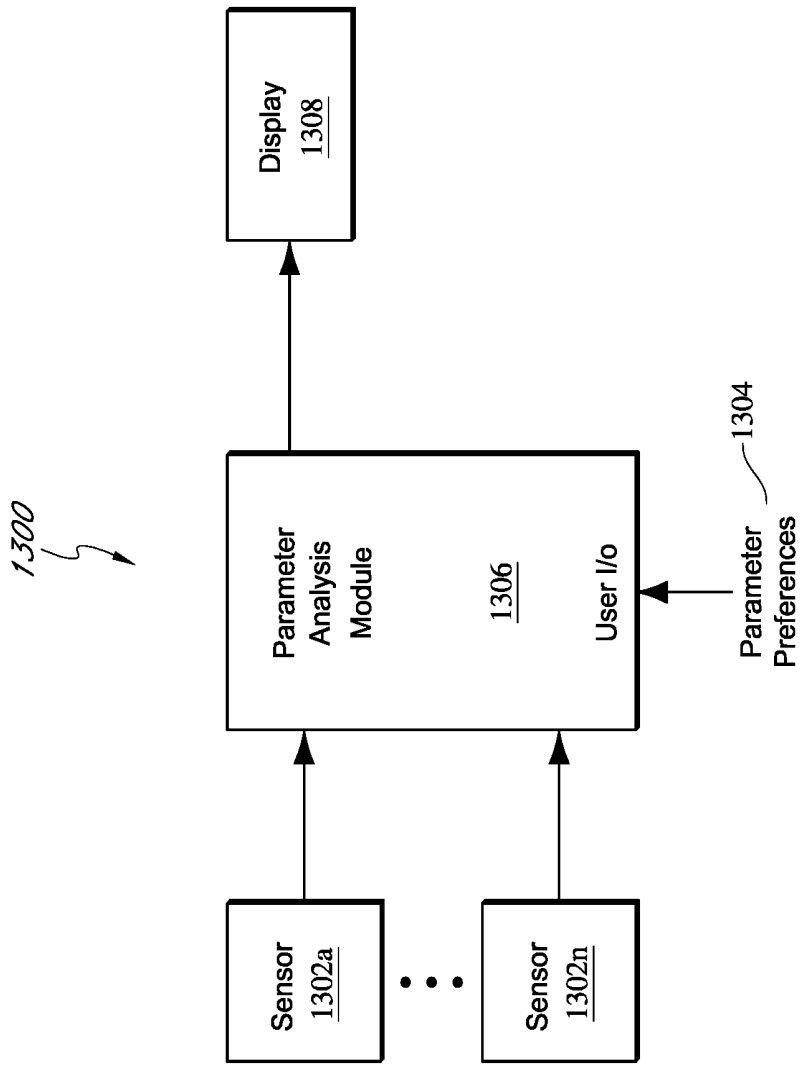

1300
Display
1308
Parameter
Analysis
Module
1306
User I/o
1304
Parameter
Preferences
Sensor
1302a
Sensor
1302n

FIG. 13

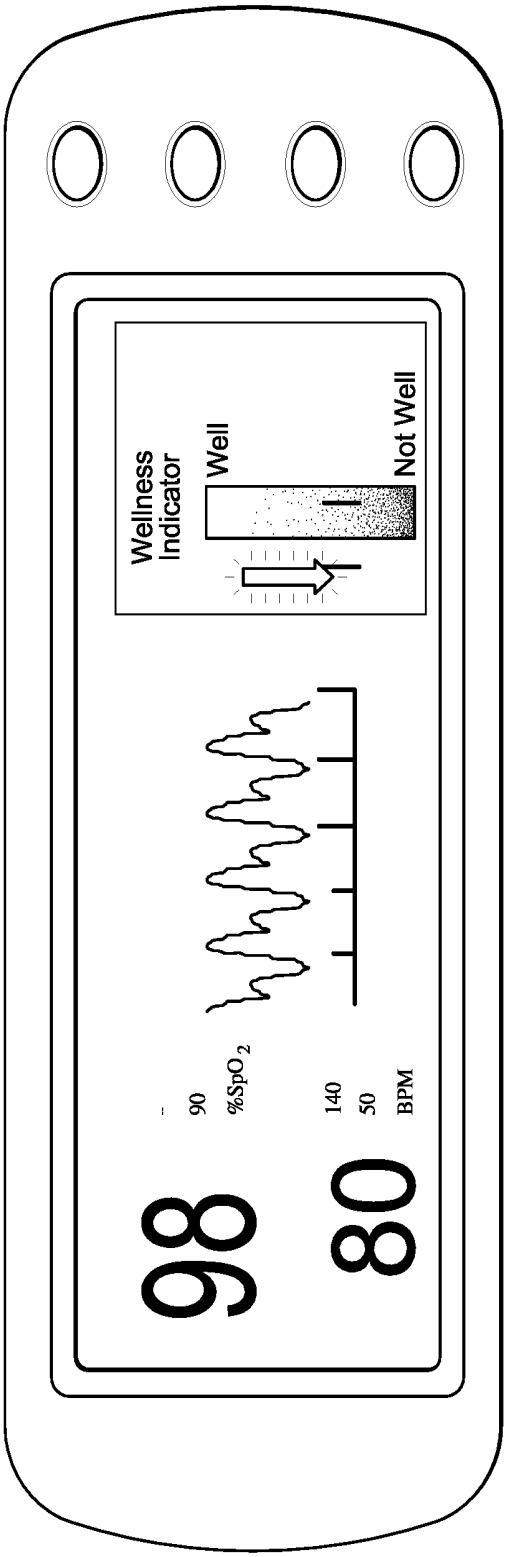


FIG. 13A

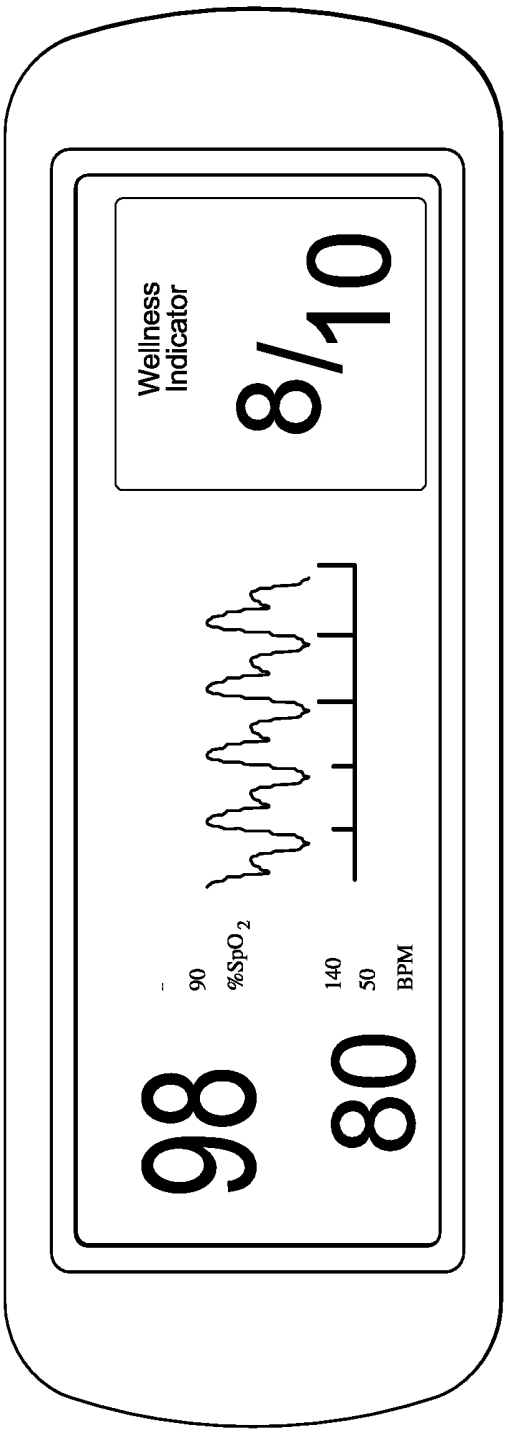


FIG. 13B

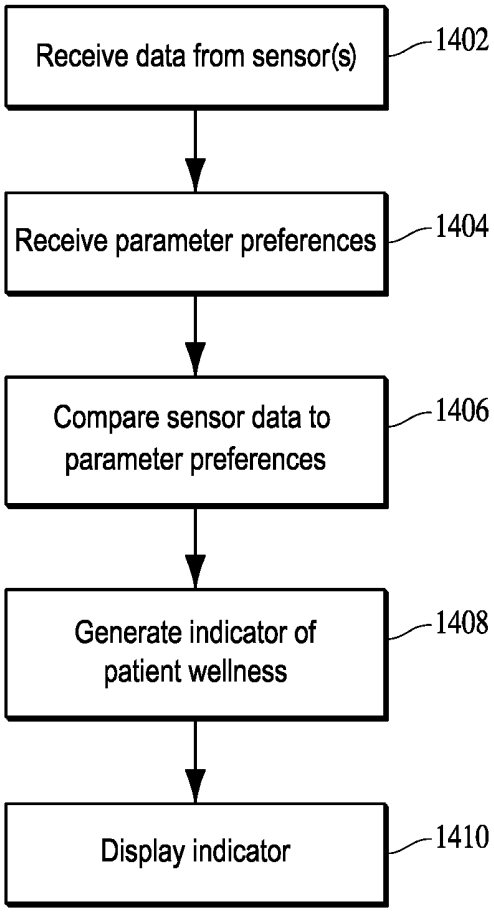

Receive data from sensor(s)
1402
Receive parameter preferences
1404
Compare sensor data to parameter preferences
1406
Generate indicator of patient wellness
1408
Display indicator
1410

FIG. 14

OPTICAL PATIENT MONITOR

PRIORITY CLAIM TO RELATED PROVISIONAL APPLICATIONS

[0001] Any and all applications for which a foreign or domestic priority claim is identified in the Application Data Sheet are hereby incorporated by reference under 37 CFR 1.57

FIELD OF THE DISCLOSURE

[0002] The present disclosure relates to a sensor for measuring physiological parameters and, in particular, relates to using measured physiological parameters to generate an indicator.

BACKGROUND

[0003] Pulse oximetry is a widely accepted noninvasive procedure for measuring the oxygen saturation level of arterial blood, an indicator of a person's oxygen supply. Early detection of a low blood oxygen level is critical in the medical field, for example in critical care and surgical applications, because an insufficient supply of oxygen can result in brain damage and death in a matter of minutes. A typical pulse oximetry system utilizes a sensor applied to a patient's finger. The sensor has an emitter configured with both red and infrared LEDs that project light through the finger to a detector so as to determine the ratio of oxygenated and deoxygenated hemoglobin light absorption. In particular, the detector generates first and second intensity signals responsive to the red and IR wavelengths emitted by the LEDs after absorption by constituents of pulsatile blood flowing within a fleshy medium, such as a finger tip. A pulse oximetry sensor is described in U.S. Pat. No. 6,088,607 titled Low Noise Optical Probe, which is assigned to Masimo Corporation, Irvine, Calif. and incorporated by reference herein.

[0004] Capnography comprises the continuous analysis and recording of carbon dioxide concentrations in the respiratory gases of patients. The device used to measure the CO_2 concentrations is referred to as a capnometer. CO_2 monitoring can be performed on both intubated and non-intubated patients. With non-intubated patients, a nasal cannula is used. Capnography helps to identify situations that can lead to hypoxia if uncorrected. Moreover, it also helps in the swift differential diagnosis of hypoxia before hypoxia can lead to irreversible brain damage. Pulse oximetry is a direct monitor of the oxygenation status of a patient. Capnography, on the other hand, is an indirect monitor that helps in the differential diagnosis of hypoxia so as to enable remedial measures to be taken expeditiously before hypoxia results in an irreversible brain damage.

[0005] Early detection of low blood oxygen is critical in a wide variety of medical applications. For example, when a patient receives an insufficient supply of oxygen in critical care and surgical applications, brain damage and death can result in just a matter of minutes. Because of this danger, the medical industry developed pulse oximetry, a noninvasive procedure for measuring the oxygen saturation of the blood. A pulse oximeter interprets signals from a sensor attached to a patient in order to determine that patient's blood oxygen saturation.

[0006] A conventional pulse oximetry sensor has a red emitter, an infrared emitter, and a photodiode detector. The sensor is typically attached to a patient's finger, earlobe, or foot. For a finger, the sensor is configured so that the emitters project light from one side of the finger, through the outer tissue of the finger, and into the blood vessels and capillaries contained inside. The photodiode is positioned at the opposite side of the finger to detect the emitted light as it emerges from the outer tissues of the finger. The photodiode generates a signal based on the emitted light and relays that signal to the pulse oximeter. The pulse oximeter determines blood oxygen saturation by computing the differential absorption by the arterial blood of the two wavelengths (red and infrared) emitted by the sensor.

SUMMARY

[0007] Multiple physiological parameters, combined, provide a more powerful patient condition assessment tool than when any physiological parameter is used by itself. For example, a combination of parameters can provide greater confidence if an alarm condition is occurring. More importantly, such a combination can be used to give an early warning of a slowly deteriorating patient condition as compared to any single parameter threshold, which may not indicate such a condition for many minutes. Conditions such as hypovolemia, hypotension, and airway obstruction may develop slowly over time. A physiological parameter system that combines multiple parameters so as to provide an early warning could have a major effect on the morbidity and mortality outcome in such cases. Parameters can include ECG, EKG, blood pressure, temperature, SpO_2, pulse rate, HbCO, HbMet, Hbt, SpaO2, HbO2, Hb, blood glucose, water, the presence or absence of therapeutic drugs (aspirin, dapson, nitrates, or the like) or abusive drugs (methamphetamine, alcohol, or the like), concentrations of carbon dioxide ("CO2"), oxygen ("O"), ph levels, bilirubin, perfusion quality, signal quality, albumin, cyanmethemoglobin, and sulfhemoglobin ("HbSulf") respiratory rate, inspiratory time, expiratory time, inspiratory to expiratory ratio, inspiratory flow, expiratory flow, tidal volume, minute volume, apnea duration, breath sounds—including rales, rhonchi, or stridor, changes in breath sounds, heart rate, heart sounds—including S1, S2, S3, S4, or murmurs, or changes in heart sounds, or the like. Some references that have common shorthand designations are referenced through such shorthand designations. For example, as used herein, HbCO designates carboxyhemoglobin, HbMet designates Methemoglobin, and Hbt designates total hemoglobin. Other shorthand designations such as COHb, MetHb, and tHb are also common in the art for these same constituents. These constituents are generally reported in terms of a percentage, often referred to as saturation, relative concentration or fractional saturation. Total hemoglobin is generally reported as a concentration in g/dL. The use of the particular shorthand designators presented in this application does not restrict the term to any particular manner in which the designated constituent is reported.

[0008] Further, a greater emphasis has been put on decreasing the pain level of patients on the ward. Accordingly, patients are often given an IV setup that enables the patient to increase the level of analgesia at will. In certain situations, however, the patient's input must be ignored so as to avoid over medication. Complications from over sedation may include hypotension, tachycardia, bradycardia, hypoventilation and apnea. A physiological parameter system that uses pulse oximetry monitoring of SpO_2 and pulse

rate in conjunction with patient controlled analgesia (PCA) can aid in patient safety. Utilization of conventional pulse oximetry in conjunction with PCA, however, can result in the patient being erroneously denied pain medication. Conventional monitors are susceptible to patient motion, which is likely to increase with rising pain. Further, conventional monitors do not provide an indication of output reliability.

[0009] Advanced pulse oximetry is motion tolerant and also provides one or more indications of signal quality or data confidence. These indicators can be used as arbitrators in decision algorithms for adjusting the PCA administration and sedation monitoring. Further, advanced pulse oximetry can provide parameters in addition to oxygen saturation and pulse rate, such as perfusion index (PI). For example, hypotension can be assessed by changes in PI, which may be associated with changes in pulse rate. Motion tolerant pulse oximetry is described in U.S. Pat. No. 6,206,830 titled Signal Processing Apparatus and Method; signal quality and data confidence indicators are described in U.S. Pat. No. 6,684,090 titled Pulse Oximetry Data Confidence Indicator, both of which are assigned to Masimo Corporation, Irvine, Calif. and incorporated by reference herein.

[0010] One aspect of a physiological parameter system is a first parameter input responsive to a first physiological sensor and a second parameter input responsive to a second physiological sensor. A processor is adapted to combine the parameters and predetermined limits for the parameters so as to generate an indication of wellness.

[0011] Another aspect of a physiological parameter system is a parameter input responsive to a physiological sensor and a quality indicator input relating to confidence in the parameter input. A processor is adapted to combine the parameter input, the quality indicator input and predetermined limits for the parameter input and the quality indicator input so as to generate a control output.

[0012] A physiological parameter method comprises the steps of inputting a parameter responsive to a physiological sensor and inputting a quality indicator related to data confidence for the parameter. A control signal is output from the combination of the parameter and the quality indicator. The control signal is adapted to affect the operation of a medical-related device.

[0013] A method of improving the reporting of a physiological parameter in a physiological parameter system comprises obtaining measurements of a physiological parameter from a measurement site. At least some of the physiological parameter measurements are maintained. A change in the measurement site is detected. A measurement of the physiological parameter from a new measurement site is obtained. The measurement of the physiological parameter at the new measurement site is compared with the maintained physiological parameter measurements. The magnitude of the physiological parameter reported by the physiological parameter system at the new measurement site is adjusted to approximately match the magnitude of the maintained physiological parameter measurements.

[0014] A method of generating an indicator of patient wellness using a physiological parameter system includes receiving physiological parameter data from a sensor attached to the physiological parameter system. Physiological parameter preferences are provided to the physiological parameter system. The physiological parameter data is compared to the physiological parameter preferences. An indicator of patient wellness is generated by calculating a numerical wellness score based on the comparison.

BRIEF DESCRIPTION OF THE DRAWINGS

[0015] FIG. **1** illustrates an embodiment of a physiological parameter measurement system.

[0016] FIG. **2**A illustrates an embodiment of a sensor assembly.

[0017] FIGS. **2**B-C illustrate alternative sensor embodiments.

[0018] FIG. **3**A illustrates an example chart of the value of a physiological parameter as measured by a sensor during a time when the sensor is moved from one measurement site to another.

[0019] FIG. **3**B illustrates a chart of a physiological parameter reported by a measurement system employing signal normalization techniques.

[0020] FIG. **3**C illustrates a chart of a MetHb reading which is smoothed to account for abnormal variations in the readings.

[0021] FIG. **3**D illustrates a MetHb smoothing flowchart.

[0022] FIG. **3**E illustrates a system of multiple different MetHb calculators which determine MetHb using different methods in order to calculate the most accurate MetHb reading.

[0023] FIG. **4** is a block diagram of a physiological parameter system having signal normalization capability.

[0024] FIG. **5** illustrates an embodiment of a method for normalizing a signal acquired by a sensor.

[0025] FIG. **6** is a general block diagram of a physiological parameter system having alarm, diagnostic and control outputs.

[0026] FIG. **6**A illustrates an embodiment of a physiological parameter system **600** similar to the system in FIG. **6**

[0027] FIG. **7** is a block diagram of a physiological parameter system combining pulse oximetry and capnography and providing alarm outputs.

[0028] FIG. **8** is a block diagram of a saturation limit alarm enhanced by $ETCO_2$ measurements.

[0029] FIG. **9** is a block diagram of a CO_2 waveform alarm enhanced by SpO_2 measurements.

[0030] FIG. **10** is a block diagram of a physiological parameter system combining pulse oximetry and capnography and providing a diagnostic output.

[0031] FIGS. **11**A, **11**B, **12** are block diagrams of a physiological parameter system utilizing pulse oximetry to control patient controlled analgesia (PCA).

[0032] FIGS. **13**, **13**A, **13**B illustrates an embodiment of a system that displays an indicator of the wellness of a patient.

[0033] FIG. **14** is a flowchart showing an example method of displaying an indicator of the wellness of a patient.

DETAILED DESCRIPTION OF PREFERRED EMBODIMENTS

[0034] Hereinafter, various example embodiments of the present disclosure will be described in detail with reference to the attached drawings such that the present disclosure can be put into practice by those skilled in the art. However, the present disclosure is not limited to the example embodiments, but may be embodied in various forms.

[0035] Some embodiments will be described in the context of computer-executable instructions, such as program modules, being executed by hardware devices, such as embedded

processors, microcontrollers, and computer workstations. Program modules may include routines, programs, objects, components, data structures, etc. that perform particular tasks or implement particular data types. Computer-executable instructions, associated data structures, and program modules represent examples of program code for executing steps of the methods disclosed herein. The particular sequence of executable instructions or arrangement of associated data structures represents examples of corresponding acts for implementing the functions described in such steps. A person of skill in the art would understand that other structures, arrangements, and executable instructions could be used with the present disclosure without departing from the spirit thereof.

[0036] FIG. **1** illustrates an embodiment of a physiological measurement system **100** having a monitor **101** and a sensor assembly **101**. The physiological measurement system **100** allows the monitoring of a person, including a patient. In particular, the multiple wavelength sensor assembly **101** allows the measurement of blood constituents and related parameters, including oxygen saturation, COHb, MetHb and pulse rate.

[0037] In an embodiment, the sensor assembly **101** is configured to plug into a monitor sensor port **103**. Monitor keys **105** provide control over operating modes and alarms, to name a few. A display **107** provides readouts of measured parameters, such as oxygen saturation, pulse rate, COHb and MetHb to name a few.

[0038] FIG. **2**A illustrates a multiple wavelength sensor assembly **201** having a sensor **203** adapted to attach to a tissue site, a sensor cable **205** and a monitor connector **201**. In an embodiment, the sensor **203** is incorporated into a reusable finger clip adapted to removably attach to, and transmit light through, a fingertip. The sensor cable **205** and monitor connector **201** are integral to the sensor **203**, as shown. In alternative embodiments, the sensor **203** can be configured separately from the cable **205** and connector **201**, although such communication can advantageously be wireless, over public or private networks or computing systems or devices, through intermediate medical or other devices, combinations of the same, or the like.

[0039] FIGS. **2**B-C illustrate alternative sensor embodiments, including a sensor **211** (FIG. **2**B) partially disposable and partially reusable (resposable) and utilizing an adhesive attachment mechanism. Also shown is a sensor **213** being disposable and utilizing an adhesive attachment mechanism. In other embodiments, a sensor can be configured to attach to various tissue sites other than a finger, such as a foot or an ear. Also a sensor can be configured as a reflectance or transflectance device that attaches to a forehead or other tissue surface. The artisan will recognize from the disclosure herein that the sensor can include mechanical structures, adhesive or other tape structures, Velcro wraps or combination structures specialized for the type of patient, type of monitoring, type of monitor, or the like.

[0040] Certain physiological parameters and certain changes in physiological parameters may serve as indicators of an adverse condition affecting a patient. For example, an increase in blood methemoglobin (MetHb) concentration may be useful as a marker of the onset of sepsis or septic shock. As another example, measurements of high blood carboxyhemoglobin (COHb) concentration may indicate exposure to carbon monoxide (CO). Other physiological and related parameters to which techniques of the present disclosure may be applicable include respiration rate, respiration volume, oxygen saturation, pulse rate, ECG, blood glucose, blood pressure, temperature, perfusion index, exhaled carbon dioxide waveform, end tidal carbon dioxide, various signal quality indicators, data confidence indicators and trend data, among others.

[0041] A sensor measuring a physiological parameter (e.g., a physiological parameter measurement device) of a patient may, under certain circumstances, detect a change in the magnitude of a detected signal that does not correspond to a change in the value of the physiological parameter. Such changes in a detected signal may occur, for example, when the sensor is moved to a different measurement site. Sometimes, a sensor may be temporarily removed from a patient, and medical reasons may compel movement of the sensor to a different location. For example, a multiple wavelength sensor may need to be moved to a different finger of a patient about every 12 hours in order to maintain the sensor's measurement effectiveness and/or to avoid injury to the patient. When the measurement site of a multiple wavelength sensor is switched to a different location, the magnitudes of some of the signals detected by the sensor may change, even though no significant change in the patient's physiological parameters has occurred during the brief sensor relocation period. Signal normalization techniques described in the present disclosure may reduce changes in physiological parameters reported by a physiological parameter system that are unrelated to actual physiological parameter variation.

[0042] In some cases, the magnitude of a sensor measurement may be a less effective indicator of an adverse condition than a change in the magnitude of a sensor measurement. In such cases, a sensor may not need to be calibrated to report the absolute magnitude of a physiological parameter when changes in the magnitude of the parameter are more significant for purposes of condition detection. In other cases, the absolute magnitude of a physiological parameter is valuable, and a sensor signal must be analyzed and/or recalibrated to compensate for changes in the magnitude of the signal detected that do not correspond to changes in the value of the physiological parameter being measured. Signal normalization techniques may improve a physiological parameter system's reporting effectiveness for both types of parameters.

[0043] FIG. **3**A illustrates an example chart **300** of the value of a physiological parameter, such as, for example, MetHb, as measured by a sensor during a time when the sensor is moved from one measurement site to another. Chart **300** shows the magnitude of a signal measured by a sensor as a function of time before any analysis or manipulation of the signal occurs. A first axis **302** of chart **300** represents time, and a second axis **304** represents the magnitude of a signal, corresponding to a physiological parameter, detected at a point in time. The physiological parameter corresponding to the signal shown by way of example in FIG. **3**A is blood MetHb concentration.

[0044] Curve **306** represents the magnitude of the signal detected by a sensor during a period when the sensor was at a first measurement site. The signal represented by curve **306** roughly oscillates about a nearly constant mean value of the signal. However, the signal may also follow any continuous increasing or decreasing trend and may also be nonoscillatory or contain a complex pattern of variation.

[0045] At time T1 along axis **302**, the sensor is removed from the first measurement site. Curve **308** represents the magnitude of the signal detected by the sensor while it is disconnected from the patient, for example, while a care provider switches the sensor to a new measurement site. In chart **300**, the magnitude of the signal is about zero, but the sensor may continue to detect a signal of some nature (e.g., random noise, background interference, etc.) during a period when it is disconnected from a patient.

[0046] At time T2 along axis **302**, the sensor is attached to a second measurement site on the patient. The second measurement site may be different than the first measurement site; for example, the second measurement site may be a different finger or a different position on a finger. Curve **310** represents the magnitude of the signal detected by the sensor during a period when the sensor is at the second measurement site. The signal represented by curve **310** roughly oscillates about a nearly constant mean value of the signal that is higher than the mean value of the portion of the signal represented by curve **306**. The difference between the magnitude of the signal shortly before time T1 and the magnitude of the signal shortly after time T2 is a shift in the magnitude of the signal that is related to the change in the measurement site. However, the shift in the signal may not correspond to an actual change in the value of a physiological parameter of the patient. In some cases, it may be safe to assume that the approximate value of a physiological parameter shortly before time T1 and shortly after time T2 is the same. In the absence of signal normalization, the signal shift may trigger a false alarm or cause a physiological parameter system to incorrectly report a change in a parameter. In the embodiment shown in FIG. **3**A, reporting the non-normalized signal may trigger an alarm for sepsis or septic shock at time T2 due to an apparent increase in blood MetHb concentration.

[0047] FIG. **3**B illustrates a chart **350** of a physiological parameter reported by a measurement system employing signal normalization techniques. In the situation corresponding to chart **350**, it is assumed that the approximate value of the physiological parameter shortly before time T1 is the same as the approximate value of the physiological parameter shortly after time T2. A first axis **352** of chart **350** represents time, and a second axis **354** represents the value of a physiological parameter reported by a physiological parameter system at a point in time. The physiological parameter shown by way of example in FIG. **3**B is blood MetHb concentration.

[0048] In chart **350**, curve **356** represents the value of the physiological parameter reported while the sensor is at the first measurement site. Curve **358** represents the value of the physiological parameter reported while the sensor is not connected to the patient. In alternative embodiments, a physiological parameter system may not report a parameter or may shut off the sensor when the system detects that the sensor is not at a measurement site. Curve **360** represents the value of the physiological parameter reported while the sensor is at the second measurement site. The physiological parameter data in chart **350** is normalized because the value of the physiological parameter reported just before T1 is adjusted to match the value of the physiological parameter just after T2. Various methods of matching may exist, including adjusting the values before and after the measurement site change to be approximately equal, using data points before T1 to generate a trend line and fixing the data point at T2 to the trend line, or any other method known in the art of projecting or approximating the value of the physiological parameter at T2 based on data prior to T1.

[0049] In some embodiments, sensor measurements that are received after time T2, as shown in curve **310** of chart **300** (FIG. **3**A), may be normalized by adding an offset to the magnitudes of the measurements. The offset may be calculated by subtracting the magnitude of the non-normalized sensor measurement at time T2 from the magnitude of the normalized sensor measurement at T2. The offset may be a negative number. Similar methods of normalizing data points involving, for example, subtraction of an offset and other known methods may also be used. One result of signal normalization is that, given a relatively constant physiological parameter over time, the mean value of curve **360** will more closely approximate the mean value of curve **356**. Signal normalization may reduce the incidence of false alarms and reports of changes in physiological parameters that have not in fact changed.

[0050] FIG. **3**C illustrates a further example of normalizing a signal with erratic noise, such as, for example, motion induced noise. As illustrated, a physiological parameter signal **370**, such as a signal indicative of MetHb, is illustrated. The physiological parameter signal **370** includes various inconsistencies, such as, for example, erratic noises **371**, probe off conditions **373**, and cite change conditions **375**. In order to deal with these inconsistencies, processing is used to determine a normalization **377** or trend of the signal. The normalization **377** uses various methods in order to determine a relatively stable physiological parameter reading **377**.

[0051] FIG. **3**D illustrates a flow chart of a normalization procedure **380**. For ease in discussion, FIGS. **3**D and **3**E will be discussed with respect to a MetHb reading, however, it should be understood that any physiological parameter can be used with the present disclosure. The normalization procedure begins with the data signal **381**. As show, the normalization feature **380** includes Met calculator **382**; smoother **384**, Met signal extractor **385**; signal quality **387** and distortion **388**. In an embodiment, a data signal **381** responsive to an intensity signal is input into the Met calculator **382**, and a current value **383** of Met is calculated. The current value **383** of Met, which in an embodiment is subject to noise, distortion, and site movements in the data signal **381**, is input into the smoother **384**, which reduces an error between the current value **383** of Met and actual MetHb conditions. For example, the smoother **384** may advantageously determine a Met trend, and depending upon an indication of some or all of an amount of distortion, noise, signal quality, and/or waveform quality in the data signal **383**, substitute or combine the MetHb trend for or with the current value **383** to generate an output MetHb measurement.

[0052] In an embodiment, the distortion signal **388** may comprise a Boolean value indicating whether the data signal **383** includes, for example, motion-induced noise. Although an artisan will recognize from the disclosure herein a number of methodologies for deriving the distortion signal **388**, derivation of a Boolean distortion signal is disclosed in U.S. Pat. No. 6,606,511, incorporated herein by reference. Alternatively, or in addition to, the signal quality signal **387** may comprise a Boolean value indicating whether the data signal **383** meets various waveform criteria Although an artisan will recognize from the disclosure herein a number of

methodologies for deriving the signal quality signal **387**, derivation of a Boolean distortion signal is disclosed in the '511 patent. Alternatively, or in addition to, a feature extractor **385** may advantageously produce waveform quality outputs **386**, indicative of waveform quality or waveform shape. Although an artisan will recognize from the disclosure herein a number of methodologies for deriving the waveform quality signal **386**, derivation thereof is disclosed in U.S. Pat. No. 6,334,065, also incorporated herein by reference.

[0053] Thus, the smoother **384** accepts one or more or different indicators of the quality of the data signal **381**, and determines how to smooth or normalize the output to reduce errors between data trends and actual MetHb conditions. In an embodiment, the smoothing may advantageously comprise statistical weighting, other statistical combinations, or simply passing the MetHb measurement **383** through to the output, depending upon one or more of the quality signals **386**, **387**, **388**, or logical combinations thereof.

[0054] Upon the output of the normalized MetHb measurement, a monitor may advantageously audibly and/or visually presents the measurement to a caregiver, and when the measurement meets certain defined thresholds or behaviors, the monitor may advantageously audibly and/or visually alert the caregiver. In other embodiments, the monitor may communicate with other computing devices to alert the caregiver, may compare longer term trend data before alarming, or the like.

[0055] FIG. **3**E illustrates a simplified block diagram of an embodiment of a MetHb determination system **390** using multiple Met calculation techniques. As shown, data **391** is input into the system. The data **391** is then routed to at least two different Met calculators **392**, **393**. In an embodiment, more than two different types of calculation techniques can be used. The at least two Met calculators **392**, **393** output Met indications for input into the Met selector **395**. The Met selector **395** determines a Met value to output. The Met selector chooses the output based on which Met calculator works best for a given condition of the signal or based on which Met calculation fits the trend of Met readings. Other methods of selecting the best Met value can also be made as would be understood by a person of skill in the art from the present disclosure.

[0056] FIG. **4** is a block diagram of a physiological parameter system having signal normalization capability. A physiological parameter system may include a sensor signal analysis subsystem **400** that implements signal normalization techniques. Signal analysis subsystem **400** receives a signal **402** from a physiological parameter measurement device output. Signal **402** may be, for example, an electrical signal produced by an optical transducer within a pulse oximeter or a capnometer.

[0057] In the embodiment shown in FIG. **4**, signal **402** is communicated to a sensor event module **404**. Sensor event module **404** includes program code for detecting events that occur based on a pattern recognized in signal **402**. Detected events may include a change in measurement site, movement of the sensor, interference in the signal, etc. For example, sensor event module **404** may determine that a measurement site of the sensor has been exchanged if a normal physiological parameter pattern ceases for a short period of time and then resumes. Alternatively, sensor event module **404** may detect a measurement site switch when signal **402** is interrupted by an interval of random noise and/or a relatively large discontinuity in the signal. Alternatively, an operator can indicate an event, such as a location change, by, for example, pressing a predetermined function button. As another example, sensor event module **404** may determine that signal normalization may not be appropriate when a sensor has been disconnected from a measurement site for a sufficiently long period of time (e.g., when an assumption that a signal trend will continue is no longer sound). Sensor event module **404** may communicate signal **402** and/or event information to a sensor memory **406** to store sensor signal pattern data for later use. Sensor event module **404** may also communicate signal **402** and event information to signal normalization module **408**.

[0058] Sensor memory **406** may retain a certain number of signal **402** samples or may retain signal **402** samples for a certain period. Retained samples may be used by program code in signal normalization module **408** and/or sensor event module **404**. Samples from signal **402** may be stored in a queue data structure, for example. In some embodiments, sensor event module **404** may instruct sensory memory **406** to cease storing new samples when it determines that the sensor is not connected to a measurement site so that signal data for potential future signal normalization may be retained. Signal memory **406** may also retain signal offset or calibration data.

[0059] Signal normalization module **408** comprises program code for converting a signal **402** from a sensor output into a normalized measure of a physiological parameter. Program code in module **408** may, for example, add or subtract a value from signal **402** in order to eliminate shifts in the magnitude of signal **402** that are not related to variation in a patient's physiological parameters. Signal normalization module **408** may determine an offset that counterbalances a shift in signal **402** that results from a change in sensor measurement site. Module **408** may include program code for calculating a trend line from data stored in sensor memory **406**. A trend line may be used to determine an appropriate value for a patient parameter when measurement resumes after an interruption in signal **402**. Module **408** may also employ pattern recognition or signal transforms to help it determine how signal **402** should be normalized. Sensor event module **404** may trigger signal normalization module **408** to reset its signal normalization when a certain signal events are detected. In some embodiments, sensor event module **404** may communicate to signal normalization module **408** the retained signal data from sensor memory **406** it should use to calculate a new offset. Signal normalization module **408** passes a normalized signal **450** out of signal normalization subsystem **400**.

[0060] Normalized signal **450** may then be passed to other components of a physiological parameter system for further analysis and/or display. For example, normalized signal **450** may be communicated to a comparator **454** that compares signal **450** to one or more parameter limits **452**. In some embodiments, comparator **454** may generate an alarm signal **456** if normalized signal **450** falls outside of parameter limits **452**.

[0061] FIG. **5** illustrates an embodiment of a method for normalizing a signal acquired by a sensor when the measurement site of the sensor is changed. At step **502**, sensor memory **406** (FIG. **4**) maintains recent physiological parameter measurements received from sensor output **402**. Sensor signal data may be passed directly to sensor memory **406** for storage, or sensor event module **404**, for example, may

select which signal samples will be retained and pass them to sensor memory **406**. Retained signal sample data may include the magnitude of the signal as well as an indicator of the time that the sample was taken and/or the order in which the sample was received. Alternatively, sensor memory **406** may simply maintain signal data in chronological order in a queue, purging old sample data as new sample data is received. Data may be retained only for a certain time interval, such several seconds, a fraction of a minute, a minute, two minutes, or longer. The interval of retention may vary depending on the physiological parameter associated with signal **402**. This step may continue until sensor event module **404** detects a sensor measurement site change.

[0062] In step **504** of FIG. **5**, sensor event module **404** detects a change in the sensor measurement site. In some embodiments, sensor event module **404** may detect the change in measurement site by one of the methods described with respect to the description of program code within sensor event module **404** above. Alternatively, a user of a physiological parameter system may indicate that a change in sensor measurement site has occurred by means of a hardware or software interface. For example, the sensor may include a hardware switch that activates when the measurement site is changed. The system may also include a manual switch or button that a user can activate to cause sensor event module **404** to register a change in the sensor measurement site. When sensor event module **404** determines that sampling at the new measurement site has begun, the method proceeds to step **506**.

[0063] At step **506**, signal normalization module **408** compares the magnitude of the signal sampled at the new measurement site with the magnitude of the retained signal that was obtained at the old measurement site. Signal normalization module **408** may use pattern recognition or signal transform techniques to attempt to compare an oscillatory signal at similar points in its cycle to obtain a more accurate comparison. In some embodiments, module **408** uses the comparison to calculate an offset that adjusts the signal at the time that measurement at the new measurement site begins to conform to a trend line fitted to signal data acquired from the old measurement site. Retained signal data from the old measurement site may be retrieved from sensor memory **406** and analyzed for the purpose of calibrating the sensor signal at the new measurement site. After the initial physiological parameter value is projected when the sensor begins sampling at the new measurement site, the method proceeds to step **508**.

[0064] In step **508**, signal normalization module **408** adjusts the magnitude of the signal measured at the new measurement site in order to output a normalized signal **450**. In some embodiments, adjusting the magnitude of the signal measured comprises modifying the magnitude of a signal measure measurement by adding or subtracting an offset. For example, the offset may be calculated by subtracting the magnitude of the signal sampled just after the sensor begins measurements at the new measurement site from the magnitude of the signal sampled just before the sensor was removed from the old measurement site. Alternatively, the offset may be defined as the difference between (1) a projected value of the magnitude of the signal just after the sensor begins measurements at the new measurement site, the projection based on measurements at the old measurement site, and (2) the actual measured value of the magnitude of the signal just after the sensor begins measurements at the new measurement site. Any other known means for calculating an offset may also be used. Signal normalization module **408** continues to add or subtract the calculated offset until another normalization step is required. At the conclusion of the method shown in FIG. **5**, the steps shown may be repeated as many times as changes in the measurement site of the sensor may require.

[0065] Various embodiments of signal normalization techniques have been shown and described. Some alternative embodiments and combinations of embodiments disclosed herein have already been mentioned. Additional embodiments comprise various other combinations or alterations of the embodiments described.

[0066] FIG. **6** illustrates a physiological parameter system **600**, which may comprise an expert system, a neural-network or a logic circuit, for example. The physiological parameter system **600** has as inputs **601** from one or more parameters from one or more physiological measurement devices, such as a pulse oximeter **610** and/or a capnometer **620**. Pulse oximeter parameters may include oxygen saturation (SpO_2), perfusion index (PI), pulse rate (PR), various signal quality and/or data confidence indicators (Qn) and trend data, to name a few. Capnography parameter inputs may include, for example, an exhaled carbon dioxide waveform, end tidal carbon dioxide ($ETCO_2$) and respiration rate (RR). Signal quality and data confidence indicators are described in U.S. Pat. No. 6,108,090 cited above. The physiological parameter system **600** may also have parameter limits **606**, which may be user inputs, default conditions or otherwise predetermined thresholds within the system **600**.

[0067] The inputs **601** are processed in combination to generate one or more outputs **602** comprising alarms, diagnostics and controls. Alarms may be used to alert medical personnel to a deteriorating condition in a patient under their care. Diagnostics may be used to assist medical personnel in determining a patient condition. Controls may be used to affect the operation of a medical-related device. Other measurement parameters **630** that can be input to the monitor may include or relate to one or more of ECG, blood glucose, blood pressure (BP), temperature (T), HbCO, MetHb, respiration rate and respiration volume, to name a few.

[0068] FIG. **6**A illustrates an embodiment of a physiological parameter system **600** similar to the system in FIG. **6**. The physiological parameter system **600** has as inputs **601** from one or more parameters from one or more physiological measurement devices, such as, for example a pulse oximeter **610**, an acoustic respiratory monitor **640**, an ECG monitor **650**, an invasive or non-invasive blood pressure monitor **650**, a thermometer, or any other invasive or non-invasive physiological monitoring devices or the like.

[0069] FIG. **7** illustrates one embodiment of a physiological parameter system **700** combining pulse oximetry parameter inputs **710** and capnography parameter inputs **720** so as to generate alarm outputs **702**. Parameter limits **705** may be user inputs, default conditions or otherwise predetermined alarm thresholds for these parameters **710**, **720**. The alarms **702** are grouped as pulse oximetry related **730**, capnography related **740** and a combination **750**. For example, a pulse oximetry alarm **730** may be related to percent oxygen saturation and trigger when oxygen saturation falls below a predetermined percentage limit. A capnography alarm **740**

may be related to $ETCO_2$ and trigger when $ETCO_2$ falls below or rises above a predetermined mm Hg pressure limit. A combination alarm **750** may indicate a particular medical condition related to both pulse oximetry and capnography or may indicate a malfunction in either instrument.

[0070] FIG. **8** illustrates a SpO_2 alarm embodiment **800** that is responsive to $ETCO_2$. In particular, a SpO_2 alarm **805** may be triggered sooner and may indicate a high priority if $ETCO_2$ **803** is falling. That is, if $ETCO_2$ **803** is trending down above a certain rate, the SpO_2 alarm **805** is triggered at a higher percentage oxygen saturation threshold and alerts a caregiver to the possibility of a serious condition, e.g. a pulmonary embolism.

[0071] As shown in FIG. **8**, a slope detector **810** determines the slope **812** of the $ETCO_2$ input **803**. A slope comparator **820** compares this slope **812** to a predetermined slope limit **804**. If the downward trend of $ETCO_2$ **803** is great enough, a delta value **803** is added **840** to the SpO_2 lower limit **802** to generate a variable threshold **842**. A threshold comparator **850** compares this variable threshold **842** to the SpO_2 input **801** to generate a trigger **852** for the SpO_2 alarm **805**. The alarm volume, modulation or tone may be altered to indicate priority, based upon the slope comparator output **822**.

[0072] FIG. **9** illustrates a CO_2 alarm embodiment **900** that is responsive to SpO_2. In particular, morphology of the input CO_2 waveform **901** is utilized to trigger an alarm **905**, and that alarm is also responsive to a falling SpO_2 **902**. That is, if a pattern in the CO_2 waveform is detected and SpO_2 is trending down above a certain rate, then an alarm is triggered. For example, an increasing slope of the CO_2 plateau in combination with a downward trend of SpO_2 may trigger an alarm and alert a caregiver to the possibility of an airway obstruction.

[0073] As shown in FIG. **9**, a pattern extractor **910** identifies salient features in the CO_2 waveform and generates a corresponding feature output **912**. A pattern memory **920** stores one or more sets of predetermined waveform features to detect in the CO_2 input **901**. The pattern memory **920** is accessed to provide a feature template **922**. A feature comparator **930** compares the feature output **912** with the feature template **922** and generates a match output **932** indicating that a specific shape or pattern has been detected in the CO_2 waveform **901**. In addition, a slope detector **940** determines the slope **942** of the SpO_2 input **902**. A slope comparator **950** compares this slope **942** to a predetermined slope limit **904**. If the downward trend of SpO_2 **902** is great enough, a slope exceeded output **952** is generated. If both the match output **932** and the slope exceeded output **952** are each asserted or "true," then a logical AND **960** generates a trigger output **96** to the alarm **970**, which generates an alarm output **905**.

[0074] FIG. **10** illustrates a combination embodiment **1000** having a diagnostic output **1005** responsive to both SpO_2 **1001** and CO_2 **1003** inputs. A SpO_2 slope detector **100** determines the slope **102** of the SpO_2 input **1001** and can be made responsive to a negative slope, a positive slope or a slope absolute value. A first comparator **1020** compares this slope **102** to a predetermined SpO_2 slope limit **1002**. If the trend of SpO_2 **1001** is great enough, a SpO_2 slope exceeded output **1022** is asserted. Likewise, an CO_2 slope detector **1030** determines the slope **1032** of the CO_2 input **1003**. A second comparator **1040** compares this slope **1032** to a predetermined CO_2 slope limit **1004**. If the downward trend of CO_2 **1001** is great enough, an CO_2 slope exceeded output **1042** is asserted. If both slope exceeded outputs **1022**, **1042** are asserted or "true," a diagnostic output **1005** is asserted.

[0075] In one embodiment, the slope detectors **610**, **1030** are responsive to a negative trend in the SpO_2 **1001** and CO_2 **1003** inputs, respectively. Accordingly, the diagnostic output **1005** indicates a potential embolism or cardiac arrest. In another embodiment, the SpO_2 slope detector **610** is responsive to negative trends in the SpO_2 **1001** input, and the CO_2 slope detector **1030** is responsive to a positive trend in the CO_2 **1003** input. Accordingly, the diagnostic output **1005** indicates a potential airway obstruction. The diagnostic output **1005** can trigger an alarm, initiate a display, or signal a nursing station, to name a few.

[0076] FIGS. **11**A-B illustrate a physiological parameter system **1100** utilizing pulse oximetry to control patient controlled analgesia (PCA). In particular embodiments, a control output **1108** is responsive to pulse oximetry parameters **1101** only if signal quality **1103** is above a predetermined threshold **1104**. In FIG. **11**A, the control output **1108** can be used to lock-out patient controlled analgesia (PCA) if pulse oximetry parameter limits have been exceeded. If signal quality is so low that those parameters are unreliable, however, PCA is advantageously allowed. That is, the pulse oximeter parameters are not allowed to lock-out PCA if those parameters are unreliable. By contrast, in FIG. **11**B, the control output **1108** can be used to advantageously lock-out or disable patient controlled analgesia (PCA) if pulse oximetry parameter limits have been exceeded or if signal quality is so low that those parameters are unreliable.

[0077] As shown in FIG. **11**A, pulse oximetry parameters **1101** and corresponding limits **1102** for those parameters are one set of inputs and a signal quality measure **1103** and a corresponding lower limit **1104** for signal quality are another set of inputs. The parameters **1101** and corresponding limits **1102** generate a combined output **1202** that is asserted if any of the pulse oximetry parameter limits are exceeded. A comparator **1110** compares the signal quality **1103** input with a lower limit **1104** generating a quality output **1112** that is asserted if the signal quality **1103** drops below that limit **1104**. An AND logic **1120** generates a reset **1122** if the combined output **1202** is asserted and the quality output **1112** is not asserted. The reset **1122** resets the timer **1130** to zero. A comparator **1140** compares the timer output **1132** to a predetermined time limit **1106** and generates a trigger **1142** if the time limit is exceeded. The trigger **1142** causes the control **1150** to generate the control output **1108**, enabling a patient controlled analgesia (PCA), for example. In this manner, the PCA is enabled if all monitored parameters are within set limits and signal quality is above its lower limit for a predetermined period of time.

[0078] As shown in FIG. **11**B, the combined output **1202**, quality output **1112**, reset **1122**, timer **1130**, comparator **1140** and control **1150** are generated as described with respect to FIG. **11**A, above. An OR logic **1121** generates a reset **1122** if either the combined output **1202** or the quality output **1112** is asserted. In this manner, the PCA is disabled for a predetermined period of time if any of the monitored parameters are outside of set limits or the signal quality is below its lower limit.

[0079] FIG. **12** illustrates combined limits **1200** having SpO_2 parameters **1101** and corresponding thresholds **1102** as inputs and providing a combination output **1202**. In particular, if any parameter **1101** exceeds its corresponding limit **1102**, the output of the corresponding comparator **1210**,

1220, **1240** is asserted. An OR logic **1250** is responsive to any asserted output **1212**, **1222**, **1242** to asserted the combined output **1202**. For example, the combined output **1202** may be asserted if SpO_2 **1201** falls below a lower limit **1209**, pulse rate (PR) **1203** rises above an upper limit **1204** or PR **1203** falls below a lower limit **120**.

[0080] A physiological parameter system has been disclosed in detail in connection with various embodiments. These embodiments are disclosed by way of examples only and are not to limit the scope of the claims that follow. One of ordinary skill in the art will appreciate many variations and modifications. For example, the control output **1108** (FIG. **11**B) can be used to control (titrate) delivered, inspired oxygen levels to patients based upon pulse oximetry parameters, unless signal quality is so low that those parameters are unreliable. One of ordinary skill in the art will also recognize that the control output **1108** (FIG. **11**B) can be used to control patient delivery of any of various pharmacological agents and/or medical gases.

[0081] FIG. **13** illustrates an embodiment of a system **1300** that displays an indicator of the wellness of a patient. Various sensors **1302***a*-**1302***n* communicate with a parameter analysis module **1306**. Sensors **1302***a*-**1302***n* may include pulse oximeters and capnometers, among other physiological parameter measurement devices. Sensor **1302***n* outputs a signal that may be sampled, normalized, and/or analyzed by modules that are not shown in system **1300** before being passed to parameter analysis module **1306**. As described above, normalization of sensor signals before comparison of the signals to parameter limits **452** (FIG. **4**) and/or parameter preferences **1304** may have certain benefits, such as decreased incidence of false alarms and/or more effective determination of the wellness of the patient.

[0082] In the embodiment shown, a user may provide parameter preferences **1304** to parameter analysis module **1306** through a user interface. Parameter preferences **1304** may include preferred ranges, less preferred ranges, least preferred ranges, upper limits, lower limits, preferred rates of increase or decrease, preferred patterns or trends, preferred states, or any combination of such preferences or other standards for evaluating the desirability of various physiological parameter values and signals. In some cases, a user of system **1300** may provide custom preferences to override a default set of physiological parameter preferences **1304** preprogrammed into system **1300**. In some embodiments, parameter analysis module **1306** may include program code for dynamically changing or suggesting changes to various parameter preferences as a function of certain physiological parameters or related sensor performance data.

[0083] Parameter analysis module **1306** compares at least some of the signal data received from sensors **1302***a*-**1302***n* to parameter preferences **1304** in order to calculate an indicator of the wellness of a patient. In some embodiments, the indicator calculated is a numerical indicator; for example, a number between one and ten, where a ten corresponds to a patient with a high level of wellness, and a one corresponds to a patient with a very low level of wellness as depicted in FIG. **13**B. Other ranges, such as one to 100, −100 to 100, etc., and scales, such as an alphabetic A-F scale or a color scale, may also be used including the scale depicted in FIG. **13**A. Other indicators that may be generated by parameter analysis module **1306** include graphical indicators of potential trouble areas, gauges, charts, level meters, and the like may also be used. Parameter analysis module **1306** communicates the indicator to a display **1308**, which may display the indicator in any suitable graphical or textual form that is known in the art. For example, display **1308** may show a number of bars or a level meter, the number of which may correspond to one of the numerical indicator scales discussed above.

[0084] FIG. **14** is a flowchart showing an example method of displaying an indicator of the wellness of a patient. At step **1402**, parameter analysis module **1306** (FIG. **13**) receives signal data from one or more sensors **1302***a*-**1302***n*. As discussed previously, such signal data may be normalized or otherwise modified from its raw form before being passed to parameter analysis module **1306**. Parameter analysis module **1306** may continuously update an indicator as new data is received and may calculate averages, variances, and/or other analytical measures of various physiological parameters over time. In some embodiments, parameter analysis module **1306** may update the indicator of patient wellness only periodically, sporadically, or by request rather than continuously, thus requiring only occasional reception of data from sensors **1302***a*-**1302***n*.

[0085] In step **1404**, parameter analysis module **1306** receives parameter preferences **1304**. Preferences **1304** may by received only once or sporadically as a user supplies custom preferences. Preferences **1304** may also be received and/or updated continuously when, for example, parameter preferences **1304** are functions of various physiological or sampling parameters.

[0086] At step **1406**, parameter analysis module **1306** compares the data received from sensors **1302***a*-**1302***n* to parameter preferences **1304**. Individual sensor measurements may be compared to parameter preferences **1304**, or parameter analysis module may compare parameter preferences **1304** to a moving average of sensor measurements, for example. Comparison of various other known analytical measures of sensor data is also possible and within the scope of the present disclosure. The comparison performed by parameter analysis module **1306** may include magnitude comparisons, pattern analysis, and/or trend analysis. Historical sensor data may also be used in the comparison.

[0087] In step **1408** of FIG. **14**, parameter analysis module **1306** generates an indicator of the wellness of the patient based on the comparison performed in step **1406**. The indicator may be in any of the forms discussed previously. For example, module **1306** may increase a wellness score (e.g., a numerical indicator of wellness) when physiological parameters fall within preferred ranges or when sensor signals follow preferred patterns and/or trends. The indicator may comprise a simple or a more detailed textual and/or graphical summary of the patient's wellness as interpreted from parameters measured by sensors **1302***a*-**1302***n*. In some embodiments, the indicator may be a scaled number in combination with a textual description of the patient's wellness score and/or conditions that may be affecting the score. In addition, particular a particular condition affecting the patient can also be generated for communication to a healthcare provider, such as, for example, sepsis, septic shock, apnea, heart failure, airway obstruction, carbon monoxide poisoning, low oxygen content, etc.

[0088] After parameter analysis module **1306** generates the wellness indicator, it sends the indicator to display **1308** at step **1410**. Display **1308** may be integrated with physi-

ological parameter system **1300** or may be a separate display device. The display may also include auditory sounds, such as for example, beeps, voices, words, etc., to indicate a particular event or condition occurring.

[0089] Although the foregoing invention has been described in terms of certain preferred embodiments, other embodiments will be apparent to those of ordinary skill in the art from the disclosure herein. Additionally, other combinations, omissions, substitutions and modifications will be apparent to the skilled artisan in view of the disclosure herein. It is contemplated that various aspects and features of the invention described can be practiced separately, combined together, or substituted for one another, and that a variety of combination and subcombinations of the features and aspects can be made and still fall within the scope of the invention. Furthermore, the systems described above need not include all of the modules and functions described in the preferred embodiments. Accordingly, the present invention is not intended to be limited by the recitation of the preferred embodiments, but is to be defined by reference to the appended claims.

1.-**26**. (canceled)

27. A method of determining a physiological parameter data through a change in measurement site, the method comprising:

obtaining first signal data from a sensor configured to attach at a first measurement site of a patient during a first time period;

determining a physiological parameter during the first time period based on the first signal data;

detecting a change in measurement site of the sensor from the first measurement site to a second measurement site of the patient;

obtaining second signal data from the second measurement site of the patient during a second time period after the first time period and after detecting the change in measurement site of the sensor;

determining an offset based on a first magnitude of a first portion of the first signal data obtained at the first measurement site and a second magnitude of a second portion of the second signal data obtained at the second measurement site;

correcting the second signal data based on the determined offset, wherein the correcting comprises shifting the second signal data based on the determined offset; and

determining the physiological parameter during the second time period based on the corrected second signal data.

28. The method of claim **27**, wherein the physiological parameter comprises a met-hemoglobin measurement.

29. The method of claim **27**, wherein the physiological parameter comprises a hemoglobin measurement.

30. The method of claim **27**, wherein the physiological parameter comprises an oxygen saturation level.

31. The method of claim **27**, wherein the determination of the offset further comprises comparing the first magnitude and the second magnitude.

32. The method of claim **27**, wherein the offset is a negative value.

33. The method of claim **27**, wherein the offset is determined by subtracting the first magnitude with the second magnitude.

34. The method of claim **27**, wherein the offset is further determined based on a projected value of the second signal data.

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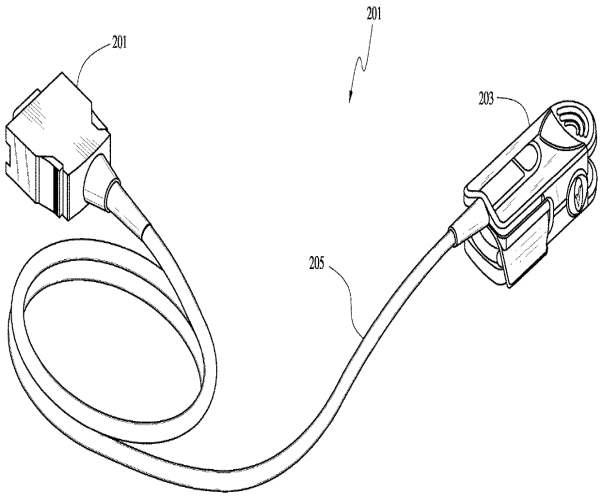
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