



US 20150150628A1

(19) **United States**

(12) **Patent Application Publication**  
**BUYSSE et al.**

(10) **Pub. No.: US 2015/0150628 A1**  
(43) **Pub. Date: Jun. 4, 2015**

(54) **THERMAL FEEDBACK SYSTEMS AND METHODS OF USING THE SAME**

**Publication Classification**

(71) Applicant: **COVIDIEN LP**, Mansfield, MA (US)

(51) **Int. Cl.**  
*A61B 18/18* (2006.01)  
*A61B 5/00* (2006.01)

(72) Inventors: **STEVEN P. BUYSSE**, NIWOT, CO (US); **CASEY M. LADTKOW**, ERIE, CO (US); **BRANDON C. GAY**, SUPERIOR, CO (US)

(52) **U.S. Cl.**  
CPC ..... *A61B 18/1815* (2013.01); *A61B 5/4836* (2013.01); *A61B 2018/1823* (2013.01); *A61B 2018/183* (2013.01); *A61B 2018/00011* (2013.01)

(21) Appl. No.: **14/618,113**

(57) **ABSTRACT**

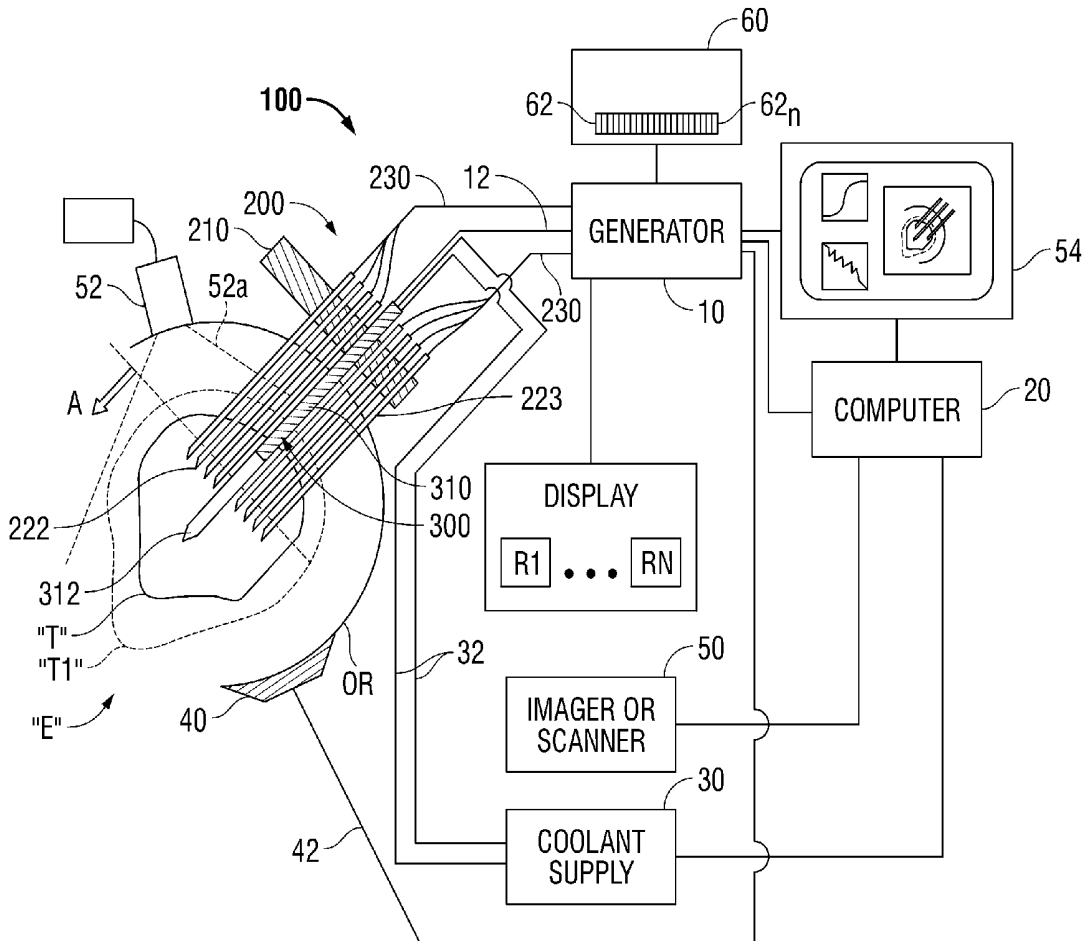
(22) Filed: **Feb. 10, 2015**

A system for providing feedback during an electrosurgical procedure on a target tissue is provided. The system includes an electrosurgical energy source; an electrode probe assembly connected to the electrosurgical energy source, wherein the electrode probe assembly includes at least one electrode assembly having a needle configured to deliver electrosurgical energy to the target tissue; at least one thermal feedback assembly connected to the electrosurgical energy source, wherein each thermal feedback assembly includes at least one temperature sensor assembly; and a hub configured to selectively support the electrode probe assembly and each thermal feedback assembly such that the needle of the electrode probe assembly and each temperature sensor assembly of each thermal feedback assembly are proximate one another when disposed proximate the target tissue.

**Related U.S. Application Data**

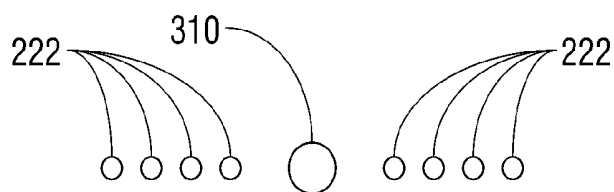
(60) Continuation of application No. 14/066,050, filed on Oct. 29, 2013, now Pat. No. 8,956,350, which is a continuation of application No. 13/539,725, filed on Jul. 2, 2012, now Pat. No. 8,568,402, which is a division of application No. 12/023,606, filed on Jan. 31, 2008, now Pat. No. 8,211,099.

(60) Provisional application No. 60/887,537, filed on Jan. 31, 2007.

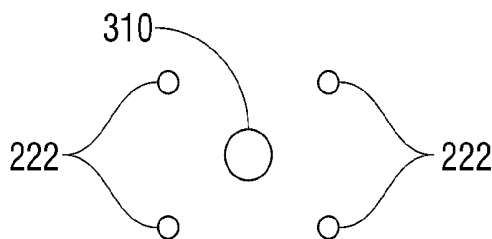




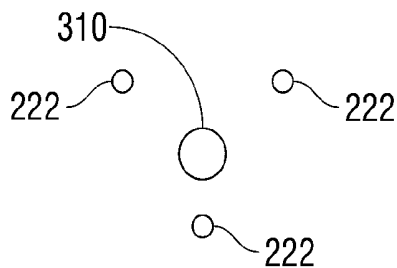




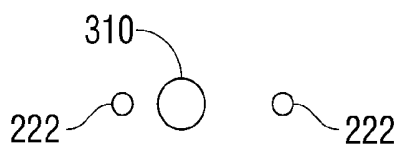
**FIG. 2A**



**FIG. 2B**



**FIG. 2C**



**FIG. 2D**

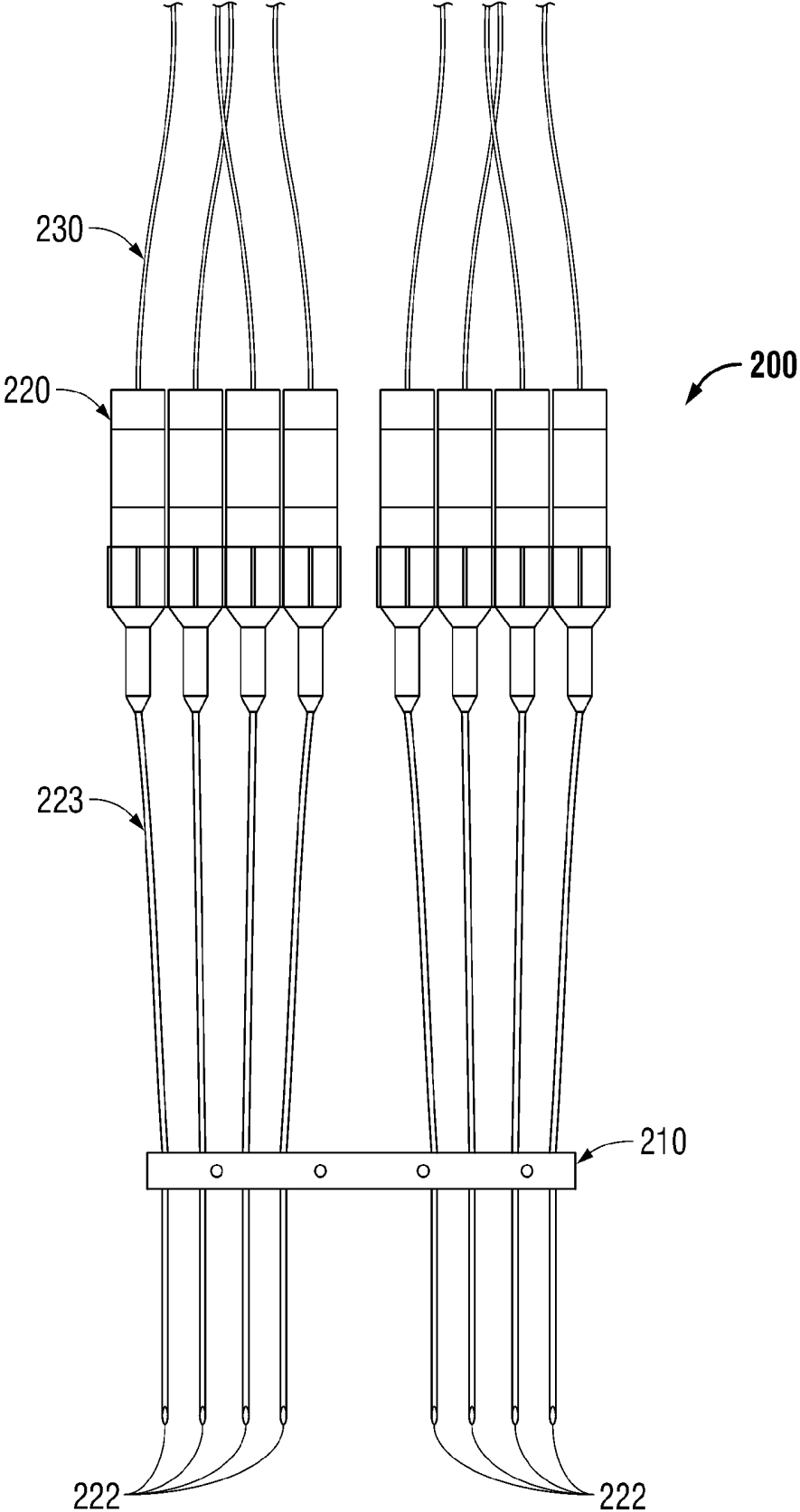


FIG. 3

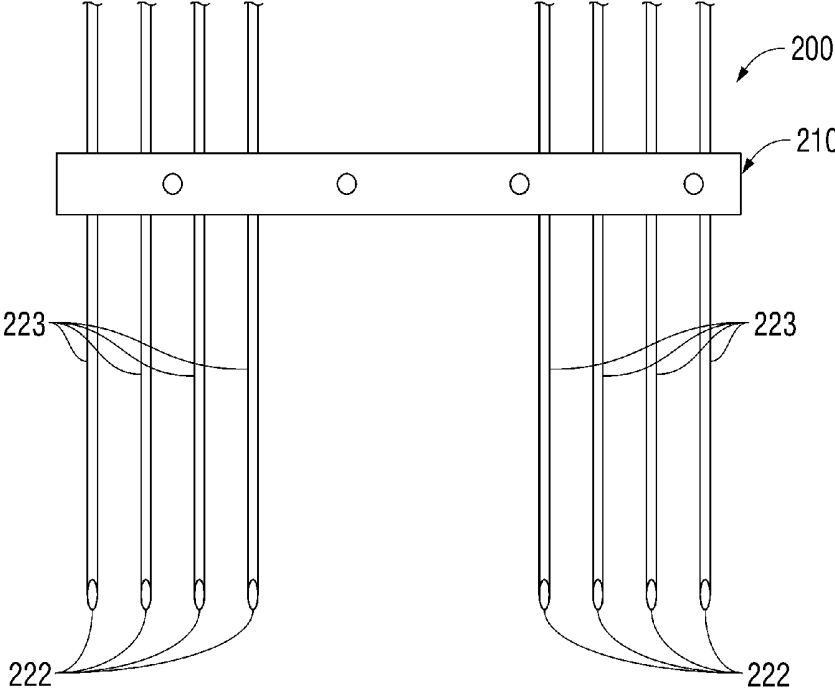


FIG. 4

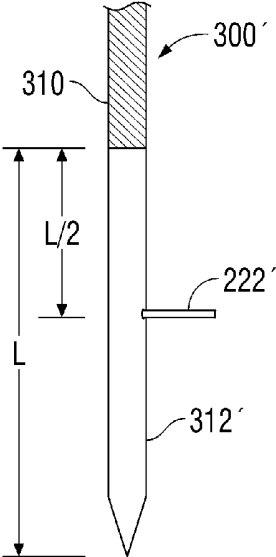


FIG. 5

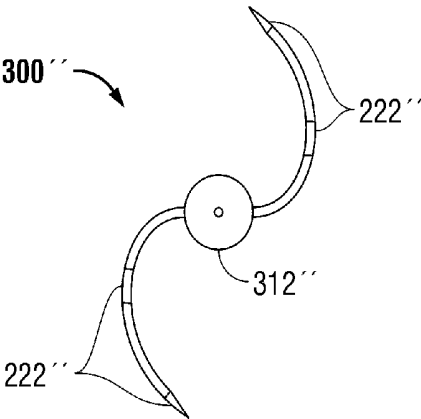


FIG. 6

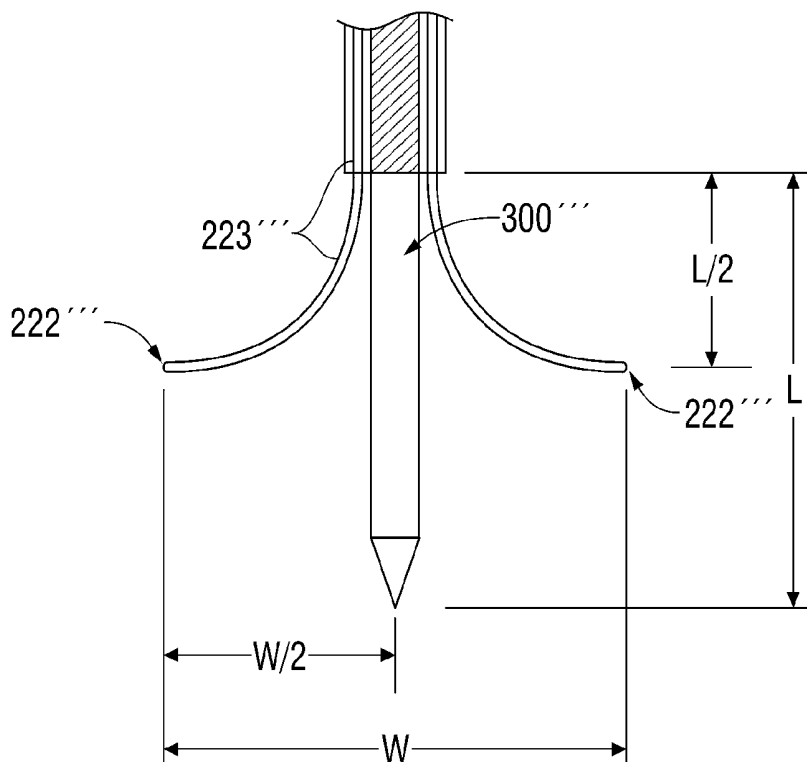


FIG. 7A

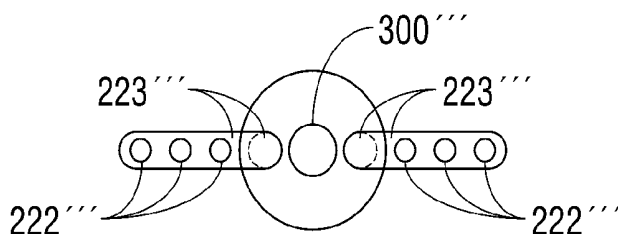


FIG. 7B

## THERMAL FEEDBACK SYSTEMS AND METHODS OF USING THE SAME

### CROSS-REFERENCE TO RELATED APPLICATIONS

[0001] The present application is a continuation application of U.S. patent application Ser. No. 14/066,050, filed Oct. 29, 2013, which is a continuation application of U.S. patent application Ser. No. 13/539,725, now U.S. Pat. No. 8,568,402, filed Jul. 2, 2012, which is a divisional application of U.S. patent application Ser. No. 12/023,606, now U.S. Pat. No. 8,211,099, filed Jan. 31, 2008, which claims the benefit of and priority to U.S. Provisional Application Ser. No. 60/887,537, filed on Jan. 31, 2007, the entire contents of all of which are incorporated by reference herein.

### BACKGROUND

[0002] 1. Technical Field

[0003] The present disclosure relates to energy delivery feedback systems and, more particularly to thermal feedback systems for electrosurgical energy systems and methods of their use.

[0004] 2. Background of Related Art

[0005] The use of electrical energy including radiofrequency and microwave energy (“RF & MW energy”) and, in particular, radiofrequency electrodes or microwave antennae (“RF-electrodes/MW-antennae”) for ablation of tissue in the body or for the treatment of pain is known. Generally, such RF electrodes (e.g., probes, resistive heating elements and the like) include an elongated cylindrical configuration for insertion into the body to target tissue which is to be treated or ablated. The RF electrodes can further include an exposed conductive tip portion and an insulated portion. The RF electrodes can also include a method of internal cooling (e.g., a Cool-Tip™ or the like), such as the RF electrodes shown and described in U.S. Pat. No. 6,506,189 entitled “COOL-TIP ELECTRODE THERMOSURGERY SYSTEM” issued to Rittman, I I I et al., on Jan. 14, 2003 and 6,530,922 entitled “CLUSTER ABLATION ELECTRODE SYSTEM” issued to Cosman et al., on Mar. 11, 2003, the entire content of which is incorporated herein by reference. Accordingly, when the RF electrode is connected to an external source of radiofrequency power, e.g., an electrosurgical generator (device used to generate therapeutic energy such as radiofrequency (RF), microwave (MW) or ultrasonic (US)), and current is delivered to the RF electrode, heating of tissue occurs near and around the exposed conductive tip portion thereof, whereby therapeutic changes in the target tissue, near the conductive tip, are created by the elevation of temperature of the tissue.

[0006] In some applications, for example, tumor ablation procedures, multiple electrodes are inserted into the body in an array to enlarge ablation volumes.

[0007] In a particular application, arrays of high frequency electrodes are inserted into tumors. The electrodes are typically placed in a dispersed fashion throughout the tumor volume to cover the tumor volume with uniform heat. The multiple electrodes may be activated simultaneously or sequentially applied with high frequency energy so that each electrode heats the surrounding tissue. During series activation, energy is applied to each electrode one at a time. This sequence of cycling the energy through the electrodes continues at a prescribed frequency and for a period of time.

[0008] The electrode systems discussed above are limited by the practical size of lesion volumes they produce. Accordingly, electrodes with cooled conductive tips have been proposed. With cooling, radiofrequency electrode tips generally produce larger lesion volumes compared with radiofrequency electrodes, which are not cooled. For example, standard single cylindrical electrodes, with cooled tips, as described above, may make lesion volumes up to 2 to 3 cm in diameter in living tissue (e.g., the liver) by using needles of 1 to 2 mm in diameter and having exposed tip lengths of several centimeters.

### SUMMARY

[0009] The present disclosure relates to thermal feedback systems for electrosurgical energy systems and methods of their use.

[0010] According to an aspect of the present disclosure, a system for providing feedback during an electrosurgical procedure on a target tissue is provided. The system includes an electrosurgical energy source; an electrode probe assembly connected to the electrosurgical energy source, wherein the electrode probe assembly includes at least one electrode assembly having a needle configured to deliver electrosurgical energy to the target tissue; at least one thermal feedback assembly connected to the electrosurgical energy source, wherein each thermal feedback assembly includes at least one temperature sensor assembly; and a hub configured to selectively support the electrode probe assembly and each thermal feedback assembly such that the needle of the electrode probe assembly and each temperature sensor assembly of each thermal feedback assembly are proximate one another when disposed proximate the target tissue.

[0011] The needle of the electrode probe assembly may include an electrically conductive distal tip electrically connected to the electrosurgical energy source.

[0012] The electrode probe assembly may be fluidly connected to a coolant supply and may be configured to receive a circulating fluid therein.

[0013] The thermal feedback assembly may include a one or more temperature sensors. Each temperature sensor may be oriented substantially parallel to an axis defined by the needle of the electrode probe assembly or protrude 90 degrees from the center exposed active electrode. The plurality of temperature sensors may be arranged in a linear array. The plurality of temperature sensors may be disposed on opposed sides of the needle of the electrode probe assembly. The plurality of temperature sensors may be uniformly spaced from one another. The plurality of temperature sensors may be arranged in one of a linear, rectilinear and a triangular array.

[0014] The system may further include a computer connected to at least one of the electrosurgical energy source, the electrode probe assembly and each thermal feedback assembly. In an embodiment, at least one of the electrosurgical or microwave generator, the electrode probe assembly and each thermal feedback assembly may transmit information to the computer, and wherein the computer performs an Arrhenius model calculation on the information received from the at least one of the electrosurgical energy source, the electrode probe assembly and each thermal feedback assembly.

[0015] The temperature sensors may include fiber optic temperature probes, thermistors, thermocouples or resistive temperature devices (RTD).

[0016] According to another aspect of the present disclosure, a method of performing a thermal treatment on a target tissue is provided. The method comprises the steps of providing an electrosurgical energy source; and providing a thermal feedback system. The thermal feedback system includes an electrode probe assembly connectable to the electrosurgical generator, wherein the electrode probe assembly includes at least one electrode assembly having a needle configured to deliver electrosurgical energy to the target tissue; at least one thermal feedback assembly connectable to the electrosurgical energy source, wherein each thermal feedback assembly includes at least one temperature sensor assembly; and a hub configured to selectively support the electrode probe assembly and each thermal feedback assembly such that the needle of the electrode probe assembly and each temperature sensor assembly of each thermal feedback assembly are proximate one another when disposed proximate the target tissue.

[0017] The method further includes the steps of inserting the needle of the electrode probe assembly and each temperature sensor of the thermal feedback assembly into a patient proximate the target tissue; activating the electrosurgical energy source for delivering electrosurgical energy to the target tissue via the needle of the electrode probe; and monitoring and transmitting changes in a characteristic of the target tissue to the electrosurgical energy source via the temperature sensors of the thermal feedback assembly.

[0018] The method may further include the step of performing an Arrhenius model calculation on the information received from each thermal feedback assembly.

[0019] The method may further include the step of selecting a particular electrode probe assembly for a particular thermal procedure or desired treatment size or volume. Size estimation may be accomplished prior to delivery of the electrode probe assembly. The method may further include the step of selecting a characteristic energy value to be delivered to the particular electrode probe assembly based on the characteristics of the electrode probe assembly and the characteristics of the target tissue to be treated.

[0020] The method may further include the step of providing feedback to the electrosurgical energy source from the plurality of thermal feedback probes. Size estimation may be conducted during energy activation.

[0021] The method may further include the step of providing a computer configured to receive information regarding characteristics of at least one of the target tissue, the feedback of energy delivery, the electrode probe assembly, the thermal feedback assembly and the electrosurgical energy source. The computer may be configured to receive feedback information from the thermal feedback assembly during a thermal treatment of the target tissue. The computer may be configured to perform an Arrhenius model calculation or other ablation size estimation on the information received from each thermal feedback assembly.

[0022] The method may further include the step of arranging the electrode probe assembly and each thermal feedback assembly in a linear array.

[0023] The method may further include the step of spacing the thermal feedback assemblies equally from each other and from the electrode probe assembly.

[0024] The method may further include the step of spacing the thermal feedback assemblies at a known or predetermined spacing.

[0025] The method may further include the step of circulating a fluid through the electrode probe assembly.

[0026] The method may further include the step of introducing the electrode probe assembly and each of the plurality of thermal feedback assemblies into the target tissue.

[0027] These and other aspects and advantages of the disclosure will become apparent from the following detailed description and the accompanying drawings, which illustrate by way of example the features of the disclosure.

#### BRIEF DESCRIPTION OF THE DRAWINGS

[0028] The features of the system and method of use of the system of the present disclosure will become more readily apparent and may be better understood by referring to the following detailed descriptions of illustrative embodiments of the present disclosure, taken in conjunction with the accompanying drawings, wherein:

[0029] FIG. 1 is a schematic illustration of a thermal feedback system illustrating an electrode probe assembly and a thermal feedback assembly of the present disclosure operatively associated with a target surgical site;

[0030] FIG. 2 is an illustration of the thermal feedback system of FIG. 1;

[0031] FIG. 2A is a schematic distal end view of the thermal feedback system of FIG. 2, illustrating the temperature array in a linear arrangement;

[0032] FIG. 2B is a schematic distal end view of an alternate arrangement of the thermal feedback system of FIG. 2, illustrating the temperature array in a rectangular arrangement;

[0033] FIG. 2C is a schematic distal end view of a further alternate arrangement of the thermal feedback system of FIG. 2, illustrating the temperature array in a triangular arrangement;

[0034] FIG. 2D is a schematic distal end view of the thermal feedback system of FIG. 2, illustrating the temperature array in an alternate linear arrangement;

[0035] FIG. 3 is an illustration of a feedback/monitoring assembly of the thermal feedback system;

[0036] FIG. 4 is an enlarged view of the indicated area of detail of FIG. 3;

[0037] FIG. 5 is a schematic illustration of a distal end of an electrode probe assembly according to a further embodiment of the present disclosure;

[0038] FIG. 6 is a distal end view of an electrode probe assembly similar to the electrode probe assembly of FIG. 5;

[0039] FIG. 7A is a schematic illustration of a distal end of an electrode probe according to an embodiment of the present disclosure; and

[0040] FIG. 7B is a distal, elevational view of the electrode probe of FIG. 7A.

#### DETAILED DESCRIPTION OF EMBODIMENTS

[0041] The systems and methods of the present disclosure provide for a more precise controlled monitoring and/or feedback of an electrode probe during therapeutic use in a target surgical site, e.g., in a cancer tumor. Moreover, the systems and methods of the present disclosure provide for an improved ability to predict and/or estimate the depth and/or volume of treatment possible by the electrode probe when the electrode probe of an electrosurgical treatment device is set to a particular or various operative parameters.

[0042] It will be readily apparent to a person skilled in the art that the systems and methods of use of the systems can be used to monitor or provide feedback during treatment of body

tissues in any body cavity or tissue locations that are accessible by percutaneous or endoscopic catheters or open surgical techniques, and is not limited to cancer tumors or the like. Application of the systems and methods in any corporal organ and/or tissue is intended to be included within the scope of the present disclosure.

[0043] 1. System for Thermal Feedback

[0044] In the drawings and in the description which follows, the term “proximal”, as is traditional, will refer to the end of the system, or component thereof, which is closest to the operator, and the term “distal” will refer to the end of the system, or component thereof, which is more remote from the operator.

[0045] With reference to FIG. 1, a thermal feedback system, according to an embodiment of the present disclosure, is generally designated as 100. Feedback system 100 includes a thermal feedback assembly 200 operatively connected to an electrosurgical generator and/or energy source 10 and/or computer 20.

[0046] At least one electrode probe assembly 300 is provided which is operatively associated with feedback assembly 200 and is connectable to electrosurgical energy source 10 in order to perform tissue ablation and the like. Each electrode probe assembly 300 may include a rigid shaft, antenna or needle 310 configured for insertion into a target tissue or organ “OR”. Needle 310 of each probe assembly 300 may terminate in an exposed distal tip 312 having a pointed configuration for facilitating percutaneous insertion of needle 310 into body organ “OR”. A portion of the external surface of needle 310 of each electrode probe assembly 300 is covered with an insulating material, as indicated by hatched line areas in FIG. 1. Distal tip 312 remains uncovered and is connected, through needle 310, to cable 12 and thereby to electrosurgical energy source 10. Electrode probe assembly 300 may include a coolant supply 30 fluidly connected to needle 310 for circulating a fluid thereto via conduit(s) 32.

[0047] Reference may be made to commonly assigned U.S. application Ser. No. 11/495,033, filed on Jul. 28, 2006, and entitled “COOL-TIP THERMOCOUPLE INCLUDING TWO-PIECE HUB” for a detailed discussion of the construction and operation of electrode probe assembly 300.

[0048] Temperatures at, or near the exposed distal tip(s) 312 of needle(s) 310 may be controlled by adjusting a flow of fluid coolant through needle 310. Accordingly, the temperature of the tissue contacting at or near distal tip(s) 312 is controlled. In operation, fluid from coolant supply 30 is carried the length of needle 310 through an inner tube (not shown) extending therethrough to the distal end of needle 310 terminating in an open end or cavity (not shown) of distal tip 312. At the opposite end of needle 310, the inner tube is connected to receive fluid. Backflow from distal tip(s) 312 is through an exit port (not shown) of needle 310.

[0049] Feedback system 100 may further include a reference electrode 40 that may be placed in contact with the skin of a patient or an external surface of organ “OR” with a connection 42 to electrosurgical energy source 10. Reference electrode 40 and connection 42 serve as a path for return current from electrosurgical energy source 10 through needle 310 of electrode probe assembly 300.

[0050] As seen in FIG. 1, by way of illustration only, a targeted region to be ablated is represented in sectional view by the line “T”. It is desired to ablate the targeted region “T” by fully engulfing targeted region “T” in a volume of lethal heat elevation. The targeted region “T” may be, for example,

a tumor which has been detected by an image scanner 50. For example, CT, MRI, fluoroscopy or ultrasonic image scanners may be used, and the image data transferred to computer 20. As an alternate example, an ultrasonic scanner head 52 may be disposed in contact with organ “OR” to provide an image illustrated by lines 52a.

[0051] For example, in FIG. 1, dashed line “T1” represents the ablation isotherm in a sectional view through organ “OR”. Such an ablation isotherm may be that of the surface achieving possible temperatures of approximately 50° C. or greater. At that temperature range, sustained for approximately 30 seconds to approximately several minutes, tissue cells will be ablated. The shape and size of the ablation volume, as illustrated by dashed line “T1”, may accordingly be controlled by a configuration of the electrode probe assemblies 300 used, the geometry of distal tips 312 of electrode probe assemblies 300, the amount of RF power applied, the time duration that the power is applied, the cooling of the needles 310 of electrode probe assemblies 300, etc.

[0052] Data processors may be connected to display devices to visualize targeted region “T” and/or ablation volume “T1” in real time during the ablation procedure.

[0053] As seen in FIG. 1, feedback system 100 may further include a library 60 including a plurality of thermal profiles/overlays 62<sub>n</sub>. As used herein, the term library is understood to include and is not limited to repository, databank, database, cache, storage unit and the like. Each overlay 62 includes a thermal profile which is characteristic of and/or specific to a particular configuration of cannula/electrode assembly or amount of exposure (i.e., specific to the length of exposure of distal tip 312 of needle 310 or the amount of needle 310 extending from a distal tip of a cannula) of the cannula/electrode assembly. In addition, for each amount of exposure or configuration of the cannula/electrode assembly, a plurality of overlays 62<sub>n</sub> is provided which includes a thermal profile which relates to, for example, the amount of time electrode probe assembly 300 is activated, to the temperature to which electrode probe assembly 300 is heated, etc.

[0054] With continued reference to FIG. 1, feedback system 100, as mentioned above, includes a thermal feedback assembly 200 operatively connected to an electrosurgical generator 10 and/or computer 20. Thermal feedback assembly 200 is operatively associated with the at least one electrode probe assembly 300.

[0055] As seen in FIG. 1, feedback assembly 200 includes a hub or housing 210 configured to selectively support at least one electrode probe assembly 300 and at least one temperature sensor assembly 220. As seen in FIG. 1, a plurality of temperature sensor assemblies 220 are shown supported in housing 210 on opposed sides of a single electrode probe assembly 300. It is contemplated that any number of temperature sensor assemblies 220 may be disposed on a single side, on opposed sides, or on multiple sides of the single electrode probe assembly 300 or relative to multiple electrode probe assemblies 300. It is further contemplated that multiple temperature sensor assemblies 220 may be interspersed amongst multiple electrode probe assemblies 300. Individual needles, cannula or introducers 223 may be used to introduce temperature sensors 222 into the target site or organ “OR”.

[0056] As seen in FIG. 2, housing 210 is used to position temperature sensor assemblies 220 on opposed sides of a single electrode probe assembly 300 so as to define a single axis or plane. Housing 210 may be configured to position cannula 223 and temperature sensors 222 of temperature

sensor assemblies 220 at a known distance from electrode probe assembly 300 and/or from one another, or are equidistant or uniformly spaced from one another.

[0057] As seen in FIG. 2A, temperature sensors 222 and electrode assembly 310 are arranged in a linear array. As seen in FIG. 2B, temperature sensors 222 and electrode assembly 310 may be arranged in a rectilinear array. As seen in FIG. 2C, temperature sensors 222 and electrode assembly 310 may be arranged in a triangular array. As seen in FIG. 2D, temperature sensors 222 are arranged at a known distance from electrode assembly 310. As seen in FIGS. 2-2D, electrode assembly 310 is located at the center of temperature sensors 222; however, electrode assembly 310 may be located at any position relative to sensors 222.

[0058] Each temperature sensor assembly 220 is electrically or optically connected to electrosurgical generator 10 via a suitable electrical connector or the like 230.

[0059] Temperature sensors 222 include one or more of an emitter, sensor or marker to provide special relationship to electrode assembly 310. Each temperature sensor assembly 220 may include a temperature sensor 222 in the form of a rigid or semi-rigid cannula 223 and/or needles configured for insertion and/or penetration into the target surgical site. Suitable temperature sensors 222 may include thermocouples, resistive temperature devices (RTD) or fiber optic temperature probes sold under the tradename "Fluoroptic® Thermometer, available from Luxtron®, Santa Clara, Calif. Temperature sensors 222 are shown and described in U.S. Pat. Nos. 4,075,497; 4,215,275; 4,448,547; 4,560,286; 4,752,141; 4,883,354; and 4,988,212.

[0060] Fluoroptic® temperature sensors 222 are configured to measure the decay time of light emitted from phosphorescent materials (e.g., phosphors). The decay time is a persistent property of the sensor that varies directly with the temperature.

[0061] Other suitable temperature sensors for use with temperature sensor assemblies 220, to measure the temperature at a target surgical site, include and are not limited to optical sensors (e.g., Fluoroptic®, infrared, etc.), thermocouples, Resistance-Temperature-Detectors (RTD), thermistors, MRI, fluoroscopic, ultrasound, CT and the like.

[0062] Temperature sensors 222 may be configured to measure or monitor temperatures greater than about 60° C. In an embodiment, feedback system 100 may be provided with suitable algorithms or the like for interpolating temperature values from at least two temperature sensors 222 and/or for integrating thermal damage from at least two temperature sensors 222. One real-time temperature sensor may be used in conjunction with an assumed or predetermined value from a look-up table or similar method.

[0063] The temperature measurements delivered to feedback system 100 may be used to generate a thermal map of the target area and/or, upon integration, may be used to account for particular tissue characteristics, such as, for example, perfusion, conduction, resistance and/or density.

[0064] In an embodiment, temperature sensors 222 may be deployed around needle 310 of the electrode probe assembly 300. Such temperature sensors may be constructed of suitable shape memory alloys so as to permit the temperature sensor to wrap around needle 310. Additionally, in an embodiment, a cannula including temperature sensors may be deployed about needle 310 of the electrode probe assembly 300. In another embodiment, as seen in FIGS. 7A and 7B, tempera-

ture sensors 222 may protrude at a substantially right angle from a center or mid point of the exposed distal tip 312 of needle 310.

[0065] Electrosurgical generator 10 and electrode probe assembly 300 may be configured to deliver energy to at least one of a radiofrequency, a microwave, an ultrasound, and a cryo-therapy needle.

[0066] Feedback system 100 is capable of providing size predictability for ablation volume to be created during a thermal procedure of a target region prior to the ablation volume exceeding a predetermined volume during the thermal procedure. For example, feedback system 100 may provide feedback regarding a volume of the thermal therapy (e.g., diameter), and estimation of an overall size of the volume of the thermal therapy, an estimation of a rate of growth of the volume of the thermal therapy, and/or an estimation of a time to completion of the thermal therapy. All of this information may be displayed on a monitor 54 (See FIG. 1) or the like. Additionally, monitor 54 may illustrate the growth of the ablation volume, in real-time, as the procedure is going forward.

[0067] As seen in FIGS. 5-7, a distal end of electrode probe assemblies according to further embodiments of the present disclosure are generally designated as 300' and 300", respectively. Electrode probe assembly 300', 300" is substantially similar to electrode probe assembly 300 and thus will only be discussed in further detail herein to the extent necessary to identify differences in construction and operation thereof.

[0068] As seen in FIGS. 5 and 7, distal tip 312' of electrode probe assembly 300' has a length of exposure "L". Additionally, electrode probe assembly 300' is configured such that temperature sensor 222' extends radially outward therefrom at a location approximately equal to "L/2". As seen in FIG. 5, temperature sensor 222' may extend radially and linearly from electrode probe assembly 300' (e.g., in a plane that is substantially orthogonal to a longitudinal axis of electrode probe assembly 300'), or, as seen in FIG. 6, temperature sensor 222" may extend radially and arcuately from electrode assembly 300" (e.g., in a plane that is substantially orthogonal to a longitudinal axis of electrode probe assembly 300").

[0069] As seen in FIG. 5, a single temperature sensor 222' may extend from electrode assembly 300', and as seen in FIG. 6, a pair of temperature sensors 222" may extend from electrode assembly 300". In any of the embodiments disclosed herein, any number of temperature sensors 222' or 222" may be used to extend from electrode assembly 300', 300" or 300".

[0070] Each temperature sensor 222' or 222" may include at least one, and as seen in FIGS. 5 and 6, a plurality of discrete respective temperature sensor elements 222a', 222a" disposed along a length thereof, such as, for example, at least at a tip thereof, at a mid-point thereof and at a base or proximal end thereof.

[0071] As seen in FIGS. 5 and 6, each temperature sensor 222' or 222" may be slidably disposed within a respective electrode probe assembly 300', 300" and configured so as to project and/or retract from within electrode probe assembly 300' or 300". Each temperature sensor 222', 222" may extend along an outer surface of a respective electrode probe assembly 300', 300".

[0072] Each temperature sensor 222', 222" may be deployable to a known and/or predetermined radial distance from respective distal tips 312', 312" of respective electrode probe assembly 310', 310". In accordance with FIG. 6, or in embodi-

ments employing multiple temperature sensors 222", the multiple temperature sensors 222" may be deployed to a known and/or predetermined distance from one another.

[0073] As seen in FIG. 7, temperature sensors 222" may be disposed to a known and/or predetermined radial distance from electrode probe assembly 300". Temperature sensors 222" are generally disposed L/2 and ½ desired diameter of thermal ablation (W/2), wherein "L" is the length of exposure of the distal end of electrode probe assembly 300" and "W" is the approximate diameter of the thermal ablation.

[0074] 2. Method for Thermal Feedback

[0075] With reference to FIGS. 1-7B, a method of using thermal feedback system 100 during the thermal treatment of a target tissue or organ "OR" with electrode probe assembly 300, 300' or 300", in conjunction with hyperthermia feedback assembly 200, is described.

[0076] A method of the present disclosure includes determining a zone of thermal treatment during and/or post treatment of the target tissue or organ "OR". The method may comprise the step of measuring a temperature of the target tissue or organ "OR", at known distances relative thereto, during and/or post treatment of the target tissue or organ "OR". The temperature of the target tissue or organ "OR", at the known distance, may be an absolute temperature and/or a temperature that is interpolated. Additionally, the method may comprise integrating the temperature over time to determine an extent of thermal treatment. Such an integration may be calculated using an "Arrhenius thermal treatment integral" or other methods of thermal damage estimation.

[0077] As used herein, "thermal damage" is a term that describes a quantity representing a relative amount of destruction to a tissue component. The component of interest can vary widely between applications from sub-cellular components, such as, for example, protein or organelles, to many celled systems, such as, for example, tumors or organs. To study systems spanning such a wide range of scale different techniques may be applied. For a relatively small system, one approach may be an "ab initio" method or some other molecular dynamic approach. For relatively larger systems, one approach may be to use an empirical method, such as, for example, the "Arrhenius" method described herein or a critical temperature criterion.

[0078] The term "Arrhenius thermal treatment" refers to a method of quantifying thermal effects on underlying tissue. The present method thus models microscopic effects in tissue, such as, for example, the denaturation of a single species of protein, or models macroscopic effects in tissue, such as, for example, a color change of the tissue associated with the thermal treatment where many different reactions have taken place.

[0079] The equation for the "Arrhenius model" may be represented by the following equation:

$$\Omega(t) = -\ln\left(\frac{c(t)}{c(0)}\right) = A \int_0^t e^{\left(\frac{-\Delta E}{RT}\right)} dt$$

[0080] where:

[0081]  $\Omega$ =is the thermal effect sustained by the tissue or organ;

[0082] c(t)=is the amount of the component of interest remaining;

[0083] c(0)=is the amount of the component of interest at time zero;

[0084] A=is the frequency factor, approximately  $7.39 \times 10^{39}$  1/s (specific to liver tissue); and

[0085]  $\Delta E$ =is the activation energy, approximately  $2.577 \times 10^5$  J/mol (specific to liver tissue).

[0086] The "Arrhenius model" is used because, in addition to combined processes, the "Arrhenius model" applies to individual processes as well. Individual processes that may be of interest include and are not limited to the denaturation of a lipid bi-layer of a cell, the denaturation of mitochondrial proteins, and the denaturation of nuclear proteins. The denaturation of lipid bi-layer is of interest because the lipid bi-layer loses its structure before many other parts of a cell. The denaturation of mitochondrial and nuclear proteins is of interest because they denature at temperatures in the range of about 42 to 60° C.

[0087] A method of the present disclosure may also include the step of using a position of electrode probe assembly 300, 300' or 300" and needle 310, positional temperature and/or feedback temperature received from hyperthermia feedback assembly 200 to determine the extent of thermal effect or treatment to the target tissue or organ "OR". The position of electrode probe assembly 300, 300' or 300" and needle 310 may be determined using a suitable positional indicator. The positional temperature may be determined by the location of temperature sensor 222, 222', 222" or 222'" and may be used to determine the presence of the lack of heat in the tissue or organ "OR".

[0088] A method of the present disclosure may also include the step of determining the spatial relationship between electrode probe assembly 300 and temperature sensor 222. Spatial relationship of electrode probe assembly 300 and temperature sensor 222 and temperature measured at temperature sensor 222 are feedback to computer 20 to determine an extent of thermal damage that may be displayed on monitor 54 or used to alter the output of electrosurgical energy source 10.

[0089] A method of the present disclosure may use a three-dimensional (3D) thermal image/map to determine a dimension of thermal treatment of the target tissue of organ "OR".

[0090] According to a method of the present disclosure, computer 20 of feedback system 100 is provided with information regarding a location of the target tissue or organ "OR", a location of critical biological structures (e.g., tissue, organs, vessels, etc.), a size and/or shape of the tumor or the target tissue or organ "OR" to be thermally treated, and a desired size of the thermal treatment volume. With this information inputted into computer 20, computer 20 may apply the "Arrhenius model" in order to develop a course of treatment.

[0091] According to a method of the present disclosure, an electrode probe assembly 300, 300' or 300" including a particular needle 310 having a given length "L" of exposure of distal tip 312 thereof is selected for a particular thermal procedure. A length "L" of electrode exposure may be user selected based on a desired volume of tissue to be treated or diameter "W" of thermal treatment. With the particular electrode probe assembly 300, 300' or 300" selected the parameters (e.g., dimensions, power rating, etc.) of electrode probe assembly 300, 300' or 300" is manually inputted or automatically selected from a look-up table for use by the electrosurgical generator 10 and/or computer 20.

[0092] With the parameters or characteristics of the tumor, target tissue or organ "OR" inputted into the electrosurgical energy source 10 and/or computer 20 and the parameters or characteristics of the electrode probe assembly 300, 300' or

**300"** selected also inputted into the electrosurgical generator **10** and/or computer **20**, the parameters of the energy to be delivered to the tumor, target tissue or organ "OR", via the electrode probe assembly **300**, **300'** or **300"**, are determined. As seen in FIG. 1, with the parameters of the energy to be delivered determined, thermal feedback assembly **200** and with electrode probe assembly **300** inserted into the patient, proximate the tumor, target tissue or organ "OR". In particular, temperature sensors **222** of thermal feedback assembly **200** and needle **310** of electrode probe assembly **300** may be inserted into the tumor, target tissue or organ "OR".

[0093] With thermal feedback assembly **200** and electrode probe assembly **300** positioned, the placement of thermal feedback assembly **200** and electrode probe assembly **300** is confirmed. Next, a spatial relationship of temperature sensors **222** and electrode probe assembly **300** may be determined by using thermal feedback assembly **200** or use of other markers, and communicated to electrosurgical energy source **10** and/or computer **20** for use of feedback control of energy parameter and/or size estimation. After confirmation of the placement of thermal feedback assembly **200** and electrode probe assembly **300** the thermal treatment of the tumor, target tissue or organ "OR" may begin. The thermal treatment of the tumor, target tissue or organ "OR" includes delivering energy produced by electrosurgical generator **10** to the tumor, target tissue or organ "OR" via electrode probe assembly **300**.

[0094] During the thermal treatment of the tumor, target tissue or organ "OR" hyperthermia feedback assembly **200** provides feedback to electrosurgical energy source **10** and/or computer **20** in the manner described above. Treatment progress is determined by computer **20** with feedback from at least one of image scanner **5**, electrosurgical energy source **10**, and temperature sensors **222**. Treatment progress is displayed on monitor **54**. Treatment progress includes one of size estimation, rate of treatment progression, and relationship of treatment volume to target volume.

[0095] While the above description contains many specific examples, these specific should not be construed as limitations on the scope of the disclosure, but merely as exemplifications of preferred embodiments thereof. Those skilled in the art will envision many other possible variations that are within the scope and spirit of the disclosure as defined by the claims appended hereto.

1-11. (canceled)

12. A system comprising:

- an electrosurgical generator configured to generate microwave energy;
- an antenna assembly configured to couple to the electrosurgical generator and deliver the generated microwave energy to tissue;
- a thermal feedback assembly operably coupled to the antenna assembly, the thermal feedback assembly configured to measure a temperature of tissue during delivery of the generated microwave energy to tissue and transmit the measured temperature to the electrosurgical generator.

13. The system according to claim 12, wherein the electrosurgical generator is further configured to control generation of microwave energy based on the measured temperature.

14. The system according to claim 12, wherein the electrosurgical generator is further configured to estimate a desired thermal treatment volume based on the measured temperature.

15. The system according to claim 12, further comprising a coolant supply fluidly coupled to the antenna assembly, the coolant fluid supply configured to circulate a coolant fluid through the antenna assembly.

16. The system according to claim 12, wherein the thermal feedback assembly is disposed on a distal portion of the antenna assembly.

17. The system according to claim 12, wherein the thermal feedback assembly is configured to measure temperature proximate a distal portion of the antenna assembly.

18. The system according to claim 12, wherein the antenna assembly includes an inner tube configured to circulate coolant fluid therethrough.

19. The system tissue according to claim 12, further comprising a hub operably coupled to the antenna assembly, the hub configured to house a portion of the antenna assembly and circulate coolant fluid therethrough.

20. The system according to claim 12, wherein the antenna assembly includes a distal radiating portion configured to deliver the generated microwave energy.

21. The system according to claim 12, wherein the thermal feedback assembly includes at least one of a temperature sensor or a thermocouple.

\* \* \* \* \*

专利名称(译)	热反馈系统及其使用方法		
公开(公告)号	<a href="#">US20150150628A1</a>	公开(公告)日	2015-06-04
申请号	US14/618113	申请日	2015-02-10
[标]申请(专利权)人(译)	柯惠有限合伙公司		
申请(专利权)人(译)	COVIDIEN LP		
当前申请(专利权)人(译)	COVIDIEN LP		
[标]发明人	BUYSSE STEVEN P LADTKOW CASEY M GAY BRANDON C		
发明人	BUYSSE, STEVEN P. LADTKOW, CASEY M. GAY, BRANDON C.		
IPC分类号	A61B18/18 A61B5/00		
CPC分类号	A61B18/1815 A61B5/4836 A61B2018/1823 A61B2018/183 A61B2018/00011 A61B2018/00702 A61B2019/5276 A61B2018/00797 A61B2018/00815 A61B2018/00821 A61B2019/5236 A61B2019/ /5238 A61B2019/524 A61B2018/00791 A61B18/1477 A61B2090/374 A61B2090/376 A61B2090/3762 A61B2090/378 A61B5/0036 A61B5/015 A61B5/743 A61B18/1206 A61B18/18		
优先权	60/887537 2007-01-31 US		
其他公开文献	US9833287		
外部链接	<a href="#">Espacenet</a> <a href="#">USPTO</a>		

摘要(译)

提供了一种用于在电外科手术期间在目标组织上提供反馈的系统。该系统包括电外科能量源;连接到电外科能量源的电极探针组件,其中电极探针组件包括至少一个电极组件,该电极组件具有构造成将电外科能量传递到目标组织的针;至少一个热反馈组件连接到电外科能量源,其中每个热反馈组件包括至少一个温度传感器组件;枢轴,被配置为选择性地支撑电极探针组件和每个热反馈组件,使得当设置在目标组织附近时,电极探针组件的针和每个热反馈组件的每个温度传感器组件彼此接近。

