



(19) **United States**
(12) **Patent Application Publication**
Werneth et al.

(10) **Pub. No.: US 2016/0192902 A1**
(43) **Pub. Date: Jul. 7, 2016**

(54) **DEVICES AND METHODS FOR DETERMINATION OF ELECTRICAL DIPOLE DENSITIES ON A CARDIAC SURFACE**

A61B 18/02 (2006.01)
A61B 18/20 (2006.01)
A61B 5/042 (2006.01)
A61B 5/0205 (2006.01)
A61B 3/113 (2006.01)
A61B 5/044 (2006.01)
A61B 5/0478 (2006.01)
A61B 5/04 (2006.01)
A61B 18/14 (2006.01)
A61B 5/0432 (2006.01)

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(52) **U.S. Cl.**
CPC *A61B 8/4416* (2013.01); *A61B 5/0432* (2013.01); *A61B 5/6805* (2013.01); *A61B 8/0883* (2013.01); *A61B 5/0452* (2013.01); *A61B 6/032* (2013.01); *A61B 8/12* (2013.01); *A61B 5/4836* (2013.01); *A61B 18/1815* (2013.01); *A61B 18/02* (2013.01); *A61B 18/20* (2013.01); *A61B 5/0422* (2013.01); *A61B 8/565* (2013.01); *A61B 5/0205* (2013.01); *A61B 3/113* (2013.01); *A61B 5/044* (2013.01); *A61B 5/0478* (2013.01); *A61B 5/04012* (2013.01); *A61B 8/464* (2013.01); *A61B 18/1492* (2013.01); *A61B 2018/00994* (2013.01)

(21) Appl. No.: **14/916,056**

(22) PCT Filed: **Sep. 10, 2014**

(86) PCT No.: **PCT/US2014/054942**

§ 371 (c)(1),

(2) Date: **Mar. 2, 2016**

Related U.S. Application Data

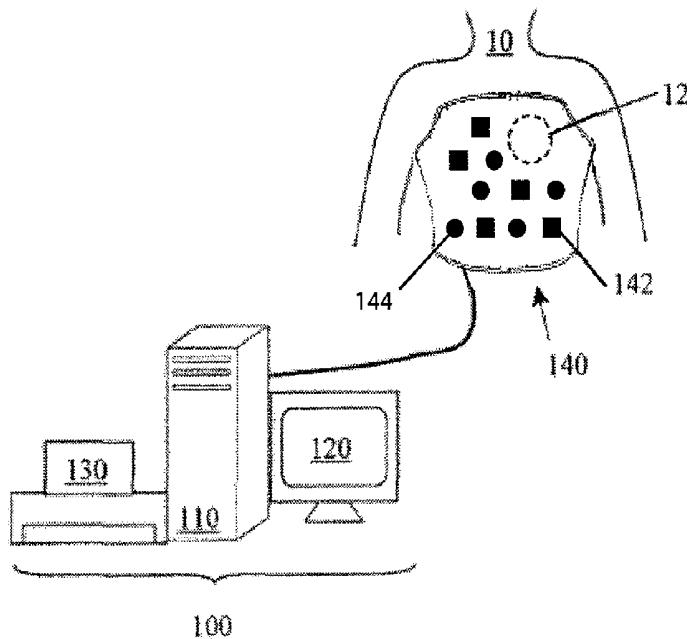
(60) Provisional application No. 61/877,617, filed on Sep. 13, 2013.

Publication Classification

(51) **Int. Cl.**
A61B 8/00 (2006.01)
A61B 5/00 (2006.01)
A61B 8/08 (2006.01)
A61B 5/0452 (2006.01)
A61B 6/03 (2006.01)
A61B 8/12 (2006.01)
A61B 18/18 (2006.01)

(57) **ABSTRACT**

Disclosed are devices, systems, and methods for determining the dipole densities on a cardiac surface using electrodes positioned on a torso of a patient. Electrodes are integrated into a piece of clothing worn by a patient. The clothing serves to fix the position of the electrodes adjacent a patient's torso. Ultrasonic transducers and sensors are used to determine a distance between the epicardial surface and the electrodes and are also used to detect epicardial surface motion as well as epicardial wall thickness.



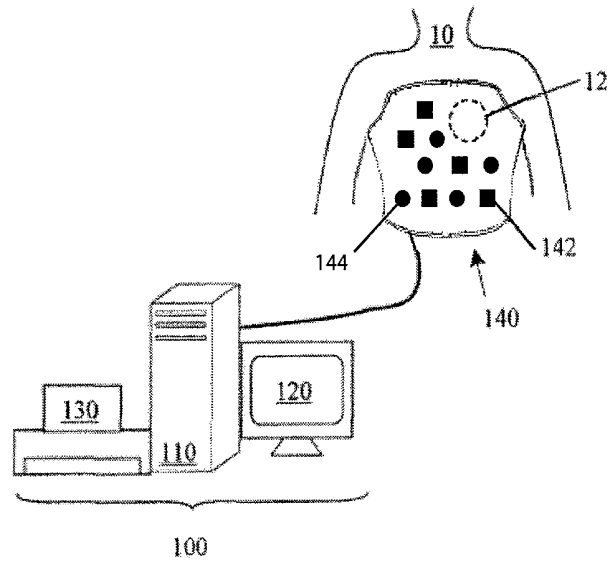


FIG. 1

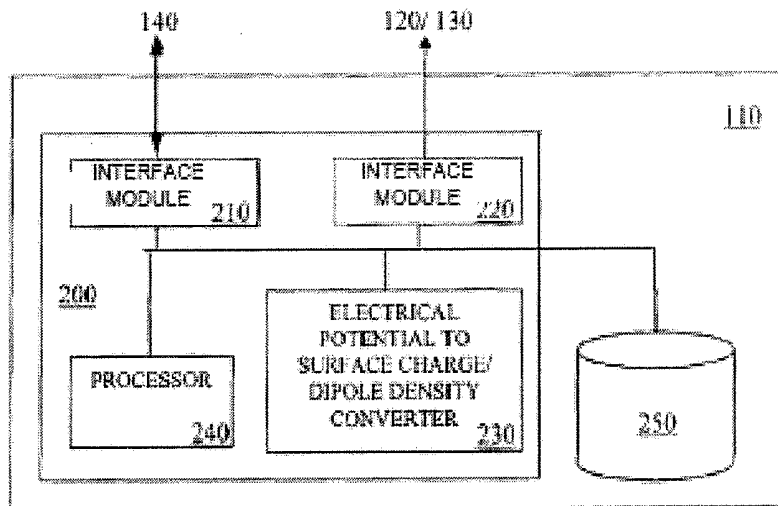


FIG. 2

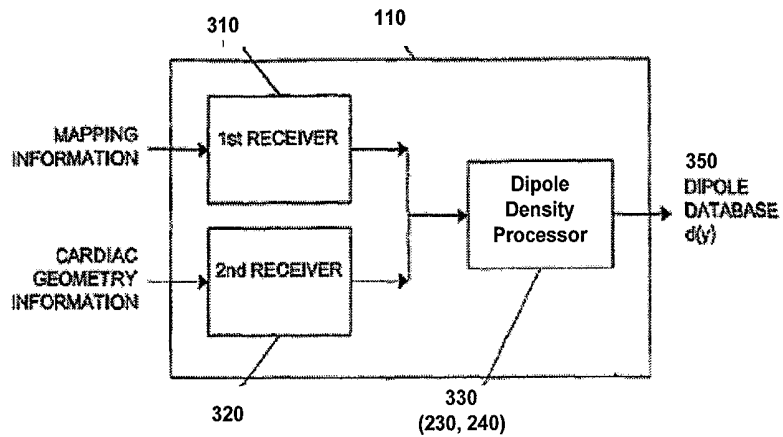


FIG. 3

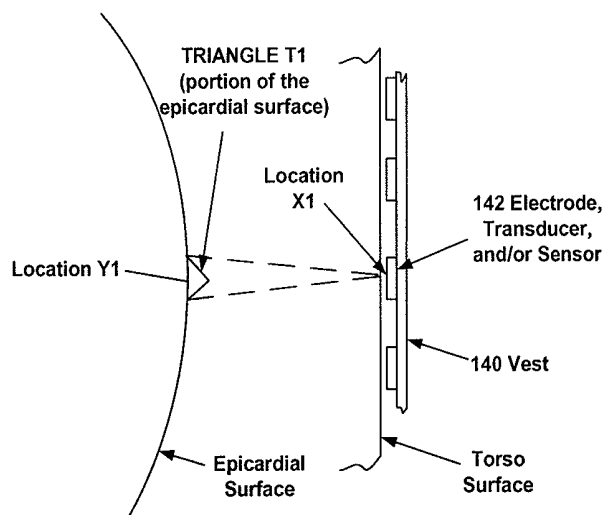


FIG. 4

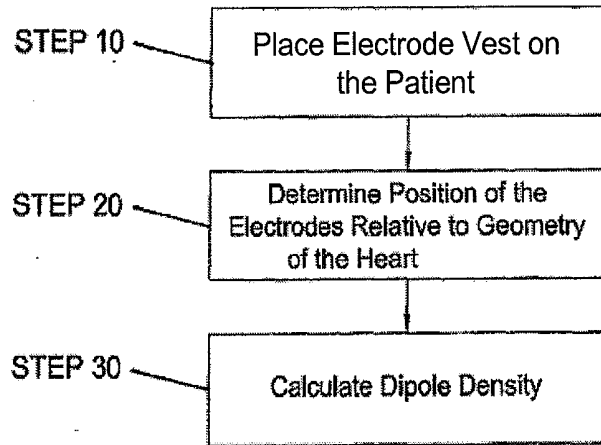
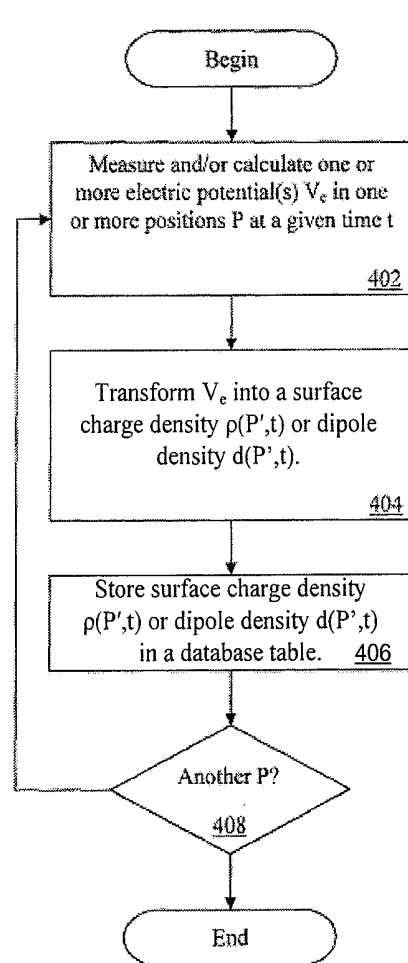


FIG. 5



400

FIG. 6

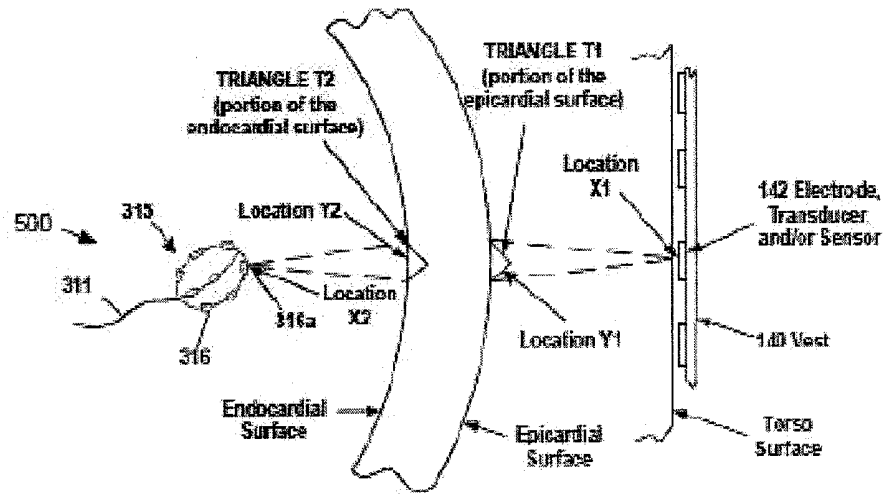


FIG. 7

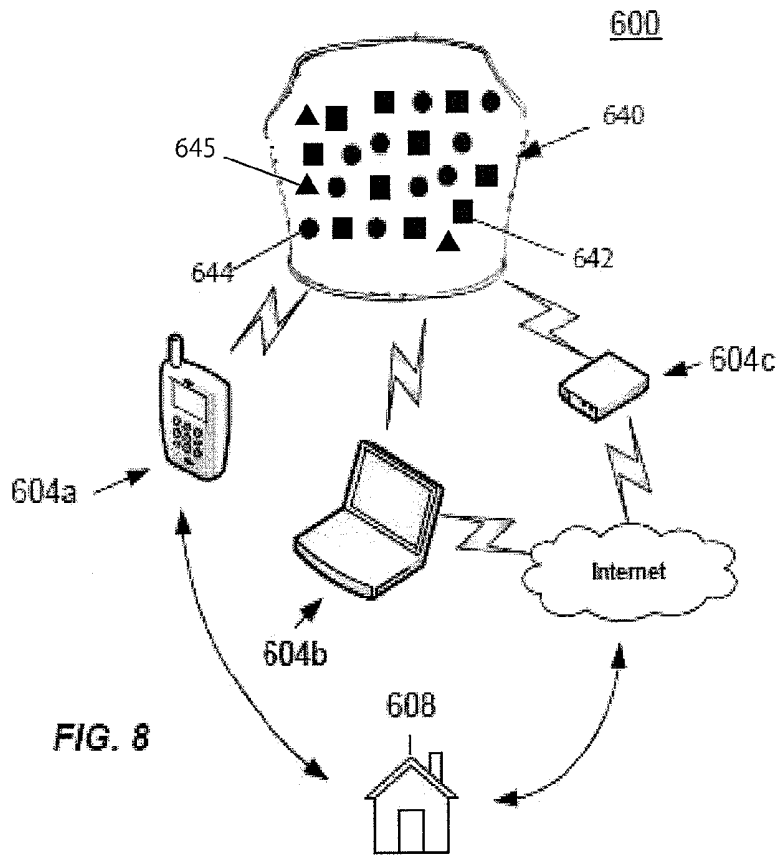


FIG. 8

**DEVICES AND METHODS FOR
DETERMINATION OF ELECTRICAL DIPOLE
DENSITIES ON A CARDIAC SURFACE**

RELATED APPLICATIONS

[0001] The present application claims priority under 35 USC 119(e) to U.S. Provisional Patent Application Ser. No. 61/877,617, entitled “Devices and Methods for Determination of Electrical Dipole Densities on a Cardiac Surface,” filed Sep. 13, 2013, which is incorporated herein by reference in its entirety.

[0002] The present application, while not claiming priority to, may be related to U.S. patent application Ser. No. 13/858,715, entitled “Method and Device for Determining and Presenting Surface Charge and Dipole Densities on Cardiac Walls”, filed Apr. 8, 2013, which is a continuation of U.S. Pat. No. 8,417,313 (hereinafter the ’313 patent), entitled “Method and Device for Determining and Presenting Surface Charge and Dipole Densities on Cardiac Walls”, issued Apr. 9, 2013, which was a 35 USC 371 national stage filing of PCT Application No. CH2007/000380, entitled “Method and Device for Determining and Presenting Surface Charge and Dipole Densities on Cardiac Walls”, filed Aug. 3, 2007, published as WO 2008/014629, which claimed priority to Swiss Patent Application No. 1251/06 filed Aug. 3, 2006, each of which is hereby incorporated by reference.

[0003] The present application, while not claiming priority to, may be related to U.S. patent application Ser. No. 13/946,712, entitled “Device and Method for the Geometric Determination of Electrical Dipole Densities on the Cardiac Wall”, filed Jul. 19, 2013, which is a continuation of U.S. Pat. No. 8,512,255, entitled “Device and Method for the Geometric Determination of Electrical Dipole Densities on the Cardiac Wall”, issued Aug. 20, 2013, published as US2010/0298690 (hereinafter the ’690 publication), which was a 35 USC 371 national stage application of Patent Cooperation Treaty Application No. PCT/IB09/00071 filed Jan. 16, 2009, entitled “A Device and Method for the Geometric Determination of Electrical Dipole Densities on the Cardiac Wall”, published as WO2009/090547, which claimed priority to Swiss Patent Application 00068/08 filed Jan. 17, 2008, each of which is hereby incorporated by reference.

[0004] The present application, while not claiming priority to, may be related to U.S. application Ser. No. 14/003,671, entitled “Device and Method for the Geometric Determination of Electrical Dipole Densities on the Cardiac Wall”, filed Sep. 6, 2013, which is a 35 USC 371 national stage filing of Patent Cooperation Treaty Application No. PCT/US2012/028593, entitled “Device and Method for the Geometric Determination of Electrical Dipole Densities on the Cardiac Wall”, published as WO2012/122517 (hereinafter the ’517 publication), which claimed priority to U.S. Patent Provisional Application Ser. No. 61/451,357, each of which is hereby incorporated by reference.

[0005] The present application, while not claiming priority to, may be related to Patent Cooperation Treaty Application No. PCT/US2013/057579, entitled “Catheter System and Methods of Medical Uses of Same, Including Diagnostic and Treatment Uses for the Heart”, filed Aug. 30, 2013, which claims priority to U.S. Patent Provisional Application Ser. No. 61/695,535, entitled “System and Method for Diagnosing and Treating Heart Tissue”, filed Aug. 31, 2012, which is hereby incorporated by reference.

[0006] The present application, while not claiming priority to, may be related to U.S. Patent Provisional Application Ser. No. 61/762,363, entitled “Expandable Catheter Assembly with Flexible Printed Circuit Board (PCB) Electrical Pathways”, filed Feb. 8, 2013, which is hereby incorporated by reference.

FIELD

[0007] The present invention is generally related to treatment of cardiac arrhythmias, and more particularly to devices and methods for dipole density mapping.

BACKGROUND

[0008] For localizing the origin(s) of cardiac arrhythmias it is common practice to measure the electric potentials located on the inner surface of the heart by electrophysiological means within the patient’s heart. One method is to insert electrode catheters into the heart to record cardiac potentials during normal heart rhythm or cardiac arrhythmia. If the arrhythmia has a regular activation sequence, the timing of the electric activation measured in voltages at the site of the electrode can be accumulated when moving the electrode around during the arrhythmia, to create a three-dimensional map of the electric activation. By doing this, information on the localization of the source of arrhythmia(s) and mechanisms, i.e., re-entry circuits, can be diagnosed to initiate or guide treatment (radiofrequency ablation). The information can also be used to guide the treatment of cardiac resynchronization, in which implantable pacing electrodes are placed in specific locations within the heart wall or chambers to re-establish a normal level of coordinated activation of the heart.

[0009] A method using external sensors measures the electrical activity of the heart from the body surface using electrocardiographic techniques that include, for example, electrocardiograms (ECG) and vectorcardiography (VCG). These external sensor techniques can be limited in their ability to provide information and/or data on regional electrocardiac activity. These methods can also fail to localize bioelectric events in the heart.

[0010] A method using external sensors for the localization of cardiac arrhythmias utilizes body surface mapping. In this technique, multiple electrodes are attached to the entire surface of the thorax and the information of the cardiac electrograms (surface ECG) is measured in voltages that are accumulated into maps of cardiac activation. This measurement can be problematic because the electrical activity is time dependent and spatially distributed throughout the myocardium and also fails to localize bioelectric events in the heart. Complex mathematical methods are required to determine the electric activation upon the outer surface of a heart model (i.e. epicardium), for instance, one obtained from CT or MRI imaging giving information on cardiac size and orientation within the thoracic cavity.

[0011] Alternatively, recordings of potentials at locations on the torso, for example, can provide body surface potential maps (BSPMs) over the torso surface. Although the BSPMs can indicate regional cardiac electrical activity in a manner that can be different from conventional ECG techniques, these BSPM techniques generally provide a comparatively low resolution, smoothed projection of cardiac electrical activity that does not facilitate visual detection or identification of cardiac event locations (e.g., sites of initiation of

cardiac arrhythmias) and details of regional activity (e.g., number and location of arrhythmogenic foci in the heart).

[0012] Since the localization of cardiac arrhythmias by the use of potentials is imprecise, the successful treatment of cardiac arrhythmias has been difficult and has demonstrated limited success and reliability. There is, therefore, a need for improved methods of localizing cardiac arrhythmias.

SUMMARY

[0013] In accordance with aspects of the present invention, provided are devices and methods for dipole density mapping, as well as methods for diagnosing tissue health. The present invention includes one or more electrodes configured to record electrical activity of tissue. In some embodiments, one or more ultrasound transducers, ultrasound sensors, and/or combinations of these can be included. The electrodes, transducers and sensors are located proximate the torso surface, and can be coupled to a wearable garment, such as a vest, shirt or bib. The device is constructed and arranged to produce continuous, real-time geometries of a patient's tissue, as well as information related to electrical activity present in the tissue.

[0014] The device can also be capable of providing tissue information, for example, tissue movement and tissue thickness. Additionally, the device can be configured to produce distance measurements by analyzing at least one of the sensors recorded angles or amplitudes or frequency changes. Non-limiting examples of distance measurements include: distance between the one or more electrodes and the epicardial surface and distance between the one or more electrodes and the one or more transducers and/or sensors.

[0015] The device can be configured to provide a tissue diagnostic through an analysis of both tissue motion information and cell electrical signals. The cell electrical signals can be recorded by the one or more electrodes, while tissue motion information can be gathered by the one or more electrodes and/or sensors. The device can be configured to provide exact foci and conduction-gap position information, such that ablation can be performed with an increased level of precision. Small conduction paths, including "gaps" in a line, are equally relevant as foci. The device can be used with an ablation device, such as robotic or manually controlled catheter ablation device. The device can also be used with a pacing system, such as a system for delivering pacing electrodes into the heart and for stimulating the heart with pacing pulses delivered through the pacing electrodes.

[0016] In accordance with one aspect of the present disclosure, a device generates a table of dipole densities $v(P,t)$ that embody an ionic nature of cellular membranes across the epicardium of a given heart of a patient. The device comprises: a measuring and recording unit that measures and records electric potential data V_e at given positions P proximate the patient's torso surface; an a/d-converter that converts the electric potential data V_e into digital voltage data; a processor that transforms the digital voltage data into cellular membrane dipole density data; and a memory that stores the electric potential data V_e and the transformed cellular membrane dipole density data.

[0017] In some embodiments, the measuring and recording unit includes multiple electrodes positioned proximate the patient's torso surface. The device can further comprise a wearable garment, and the multiple electrodes can be coupled to the wearable garment. The wearable garment can be flexible and conform closely to the patient's torso surface. The

wearable garment can be configured to urge the multiple electrodes against the torso surface with a consistent position to prevent movement of at least one of the multiple electrodes.

[0018] In various embodiments, the wearable garment can be selected from the group consisting of: vest; shirt; bib; arm band; torso band; any patient-attachable assembly capable of maintaining the one or more electrodes in contact with the torso surface or sufficiently close thereto that a monitorable signal is detectable; and/or combinations thereof.

[0019] In some embodiments, the processor executes a computer program embodying an algorithm for transforming the digital voltage data into cellular membrane dipole density data. The computer program can be stored in a storage device, e.g., an electrical, magnetic, and/or optical storage device. The storage device can be a non-transitory storage device.

[0020] In some embodiments, the device further comprises one or more ultrasound transducers positioned proximate the patient's torso surface, the one or more ultrasound transducers being configured to emit waves toward an epicardial surface; and one or more ultrasound sensors positioned proximate the patient's torso surface, the one or more ultrasound sensors being configured to receive reflections of the waves from the epicardial surface and produce sensor data. The processor can be configured to receive the sensor data from the one or more sensors and generate distance measurements from the epicardial surface. The processor can be configured to produce the distance measurements by analyzing at least one of: timing of received signal; recorded signal amplitude; sensor recorded angle; or signal frequency changes.

[0021] The device can further comprise at least one wearable garment, and the at least one of the multiple electrodes, one or more ultrasound transducers, or one or more ultrasound sensors can be coupled to the at least one wearable garment. The at least one wearable garment can comprise a first wearable garment and a second wearable garment, and the multiple electrodes can be coupled to the first wearable garment, and the one or more ultrasound transducers and one or more ultrasound sensors can be coupled to the second wearable garment. In various embodiments, the at least one wearable garment can be selected from the group consisting of: vest; shirt; bib; arm band; torso band; any patient-attachable assembly capable of maintaining the one or more electrodes, one or more ultrasound transducers, and/or one or more ultrasound sensors in contact with the torso surface, or sufficiently close thereto that a monitorable signal is detectable; and/or combinations thereof.

[0022] In some embodiments, the device can be configured to diagnose at least one of: an arrhythmia; ischemia; or compromised myocardial function.

[0023] In some embodiments, the device can be configured to treat at least one of: an arrhythmia; ischemia; or compromised myocardial function.

[0024] In accordance with another aspect of the present disclosure, a device for creating a database of dipole densities $d(y)$ at an epicardial surface of the heart of a patient comprises: multiple electrodes positioned proximate the patient's torso surface; a first receiver configured to receive mapping information from the multiple electrodes; a second receiver configured to receive an anatomical depiction of the heart; a dipole density module configured to generate the database of dipole densities $d(y)$ of polygonal shaped projections onto the epicardial surface, wherein the dipole density module computes the dipole density at all vertices of the polygonal shaped projections, wherein if the dipole density is $d(y)$, the total

measured potential $V(x)$ at a location x is the sum over all vertices of $d(y)$ times a matrix $\omega(x,y)$, and wherein: a) x represents a series of locations on the torso surface; and b) $V(x)$ is a measured potential at point x , said measured potential recorded by the multiple electrodes.

[0025] In some embodiments, the dipole density module can generate the database of dipole densities $d(y)$ using a finite elements method.

[0026] In some embodiments, the polygonal shaped projections can be substantially the same size.

[0027] In some embodiments, the dipole density can be determined by a number of polygonal shaped projections, wherein the number can be determined by the size of the epicardial surface.

[0028] In some embodiments, the polygonal shaped projections can be selected from the group consisting of: triangles; squares; tetrahedral shapes; hexagonal shapes; any other suitable shape compatible with finite elements method; and/or combinations thereof.

[0029] In some embodiments, the device can further comprise a wearable garment, and the multiple electrodes can be coupled to the wearable garment. The wearable garment can be flexible and conform closely to the patient's torso surface. The wearable garment can be configured to urge the multiple electrodes against the torso surface with a consistent position to prevent movement of the electrodes. The wearable garment can be selected from the group consisting of: vest; shirt; bib; arm band; torso band; any patient-attachable assembly capable of maintaining the one or more electrodes in contact with the torso surface or sufficiently close thereto that a monitorable signal is detectable; and/or combinations thereof.

[0030] In some embodiments, the anatomical depiction of the heart can comprise previous anatomical imaging and/or real-time anatomical imaging from one or more of CT; MRI; internal ultrasound; external ultrasound; or other imaging apparatus.

[0031] In some embodiments, the anatomical depiction of the heart can comprise a generic model of a heart.

[0032] In some embodiments, the device can further comprise: one or more ultrasound transducers positioned proximate the patient's torso surface, the one or more ultrasound transducers being configured to emit waves toward the epicardial surface; and one or more ultrasound sensors positioned proximate the patient's torso surface, the one or more ultrasound sensors being configured to receive reflections of the waves from the epicardial surface.

[0033] The device can further comprise at least one wearable garment, and at least one of the multiple electrodes, one or more ultrasound transducers, and/or one or more ultrasound sensors can be coupled to the at least one wearable garment. The at least one wearable garment can comprise a first wearable garment and a second wearable garment, and the multiple electrodes can be coupled to the first wearable garment, and the one or more ultrasound transducers and/or one or more ultrasound sensors can be coupled to the second wearable garment. The at least one wearable garment can be selected from the group consisting of: vest; shirt; bib; arm band; torso band; any patient-attachable assembly capable of maintaining the one or more electrodes, one or more ultrasound transducers, and/or one or more ultrasound sensors in contact with the torso surface, or sufficiently close thereto that a monitorable signal is detectable; and/or combinations thereof. The anatomical depiction of the heart can comprise

real-time anatomical imaging from the one or more ultrasound transducers and the one or more ultrasound sensors.

[0034] In some embodiments, the device can be configured to diagnose at least one of: an arrhythmia; ischemia; or compromised myocardial function.

[0035] In some embodiments, the device can be configured to treat at least one of: an arrhythmia; ischemia; or compromised myocardial function.

[0036] In accordance with another aspect of the present disclosure, a method of creating a database of dipole densities $d(y)$ at the epicardial surface of the heart of a patient comprises: placing an array of multiple electrodes proximate the patient's torso surface; and calculating dipole densities $d(y)$ by: receiving mapping information from the multiple electrodes; receiving an anatomical depiction of the heart; and generating the database of dipole densities $d(y)$ with a dipole density module, wherein the dipole density module determines dipole densities $d(y)$ of polygonal shaped projections onto the epicardial surface, wherein the dipole density module computes the dipole density at all vertices of the polygonal shaped projections, wherein if the dipole density is $d(y)$, the total measured potential $V(x)$ at a location x is the sum over all vertices of $d(y)$ times a matrix $\omega(x,y)$, and wherein: a) x represents a series of locations on the torso surface; and b) $V(x)$ is a measured potential at point x , said measured potential recorded by the multiple electrodes.

[0037] In some embodiments, the dipole density module can generate the database of dipole densities $d(y)$ using a finite elements method.

[0038] In some embodiments, the method can further comprise providing a wearable garment, and the multiple electrodes can be coupled to the wearable garment. The wearable garment can be configured to urge the multiple electrodes against the torso surface with a consistent position to prevent movement of the electrodes. The wearable garment can be selected from the group consisting of: vest; shirt; bib; arm band; torso band; any patient-attachable assembly capable of maintaining the one or more electrodes in contact with the torso surface or sufficiently close thereto that a monitorable signal is detectable; and/or combinations thereof.

[0039] In some embodiments, the method can include using the dipole densities $d(y)$ to locate an origin of abnormal electrical activity of a heart.

[0040] In some embodiments, the method can include using the dipole densities $d(y)$ to diagnose at least one of: an arrhythmia; ischemia; or compromised myocardial function.

[0041] In some embodiments, the method can include using the dipole densities $d(y)$ to treat at least one of: an arrhythmia; ischemia; or compromised myocardial function.

[0042] In some embodiments, calculating the dipole densities $d(y)$ can include a processor executing a computer program stored in a memory, the computer program embodying an algorithm for generating a table of dipole densities in the memory. The memory can be a non-transitory storage device, such as an electrical, magnetic, and/or optical storage device, as examples.

[0043] In accordance with another aspect of the present disclosure, a device for creating a database of dipole densities $d(y)$ and distance measurements at an epicardial surface of a patient comprises: an array of multiple electrodes positioned proximate the patient's torso surface; one or more ultrasound transducers positioned proximate the patient's torso surface, the one or more ultrasound transducers being configured to emit waves toward the epicardial surface; one or more ultra-

sound sensors positioned proximate the patient's torso surface, the one or more ultrasound sensors being configured to receive reflections of the waves from the epicardial surface; and a computer coupled to the multiple electrodes, one or more ultrasound transducers, and one or more ultrasound sensors, wherein the computer is configured to receive mapping information from the multiple electrodes and sensor data from the one or more sensors, and generate the database of dipole densities $d(y)$ and distance measurements.

[0044] In some embodiments, the device can further comprise at least one wearable garment, and at least one of the multiple electrodes, one or more ultrasound transducers, and/or one or more ultrasound sensors can be coupled to the at least one wearable garment. The wearable garment can be flexible and conform closely to the body of the patient. The wearable garment can be configured to urge electrodes, sensors and/or transducers against the torso surface with a consistent position to prevent movement of the electrodes, sensors and/or transducers. The at least one wearable garment can be selected from the group consisting of: vest; shirt; bib; arm band; torso band; any patient-attachable assembly capable of maintaining the one or more electrodes, one or more ultrasound transducers, and one or more ultrasound sensors in contact with the torso surface, or sufficiently close thereto that a monitorable signal is detectable; and combinations thereof.

[0045] In various embodiments, the at least one wearable garment can comprise a first wearable garment and a second wearable garment, and the multiple electrodes can be coupled to the first wearable garment, and the one or more ultrasound transducers and/or one or more ultrasound sensors can be coupled to the second wearable garment. The computer can be coupled to the wearable garment.

[0046] In some embodiments, the computer can include: a dipole density module configured to generate a three dimensional database of dipole densities $d(y)$, and wherein the dipole density module determines a dipole density for polygonal shaped projections onto the epicardial surface and computes the dipole density at all vertices of the polygonal shaped projections, wherein if the dipole density is $d(y)$, the total measured potential $V(x)$ at a location x is the sum over all vertices of $d(y)$ times a matrix $\omega(x,y)$, and wherein: a) x represents a series of locations on the torso surface; and b) $V(x)$ is a measured potential at point x , said measured potential recorded by the multiple electrodes. The dipole density module can generate the database of dipole densities $d(y)$ using a finite elements method. The polygonal shaped projections can be substantially the same size. The dipole density can be determined by a number of polygonal shaped projections, the number determined by the size of an epicardial surface. Such module can include or be embodied in, as examples, hardware, computer program code, firmware, and/or combinations thereof.

[0047] In some embodiments, the device can be configured to provide epicardial surface motion information of the heart. The device can be configured to provide tissue diagnostic information by analyzing both motion information and cell electrical signals. The cell electrical signals can be recorded by the multiple electrodes.

[0048] In some embodiments, the device can further include a display configured to display real time motion.

[0049] In some embodiments, the computer can be configured to produce a geometrical depiction of the heart.

[0050] In some embodiments, the device can be further configured to determine properties of the cardiac wall. The properties can include cardiac wall thickness information. The properties can include precise foci, conduction-gaps, and/or conduction channels position information.

[0051] In some embodiments, the distance measurement can comprise the distance between at least one of the multiple electrodes and at least one epicardial surface.

[0052] In some embodiments, the device can be configured to produce the distance measurement by analyzing at least one of: timing of received signal; recorded signal amplitude; sensor recorded angle; or signal frequency changes.

[0053] In some embodiments, the device can be configured to provide epicardial surface information during a cardiac ablation procedure. The ablation procedure can comprise delivery of RF, ultrasound, microwave, cryogenic and/or laser energy to tissue.

[0054] In some embodiments, at least one of the sensors and at least one of the transducers can comprise a single component.

[0055] In some embodiments, at least one of the sensors and at least one of the transducers can be integral to at least one electrode of the multiple electrodes.

[0056] In some embodiments, the computer can be configured to determine a map of dipole densities $d(y)$ at corresponding time intervals.

[0057] In some embodiments, the computer can be configured to generate a synthesis of maps that represents a cascade of activation sequences of each corresponding heart beat from a series of heart beats.

[0058] In some embodiments, the device can be configured to diagnose at least one of: an arrhythmia; ischemia; or compromised myocardial function.

[0059] In some embodiments, the device can be configured to treat at least one of: an arrhythmia; ischemia; or compromised myocardial function.

[0060] In accordance with another aspect of the present disclosure, a method of creating a database of dipole densities $d(y)$ and distance measurements at an epicardial surface of a patient comprises: placing an array of multiple electrodes, one or more ultrasound transducers, and one or more ultrasound sensors proximate the patient's torso surface; and calculating dipole densities $d(y)$ by: receiving mapping information from the multiple electrodes; emitting waves toward the epicardial surface with the one or more ultrasound transducers; receiving reflections of the waves from the epicardial surface with the one or more ultrasound sensors; producing a geometrical depiction of the epicardial surface; generating the database of dipole densities $d(y)$ with a dipole density module, wherein the dipole density module determines dipole densities $d(y)$ of polygonal shaped projections onto the epicardial surface, wherein the dipole density module computes the dipole density at all vertices of the polygonal shaped projections, wherein if the dipole density is $d(y)$, the total measured potential $V(x)$ at a location x is the sum over all vertices of $d(y)$ times a matrix $\omega(x,y)$, and wherein: a) x represents a series of locations on the torso surface; and b) $V(x)$ is a measured potential at point x , said measured potential recorded by the multiple electrodes; and calculating distance or movement information by analyzing signals received from the sensor.

[0061] In some embodiments, the dipole density module can be configured to generate the database of dipole densities $d(y)$ using a finite elements method.

[0062] In some embodiments, the method can further comprise providing at least one wearable garment, wherein at least one of the multiple electrodes, one or more ultrasound transducers, and one or more ultrasound sensors can be coupled to the at least one wearable garment. The at least one wearable garment can be configured to urge the electrodes, sensors and/or transducers against the torso surface with a consistent position to prevent movement of the electrodes, sensors and/or transducers. The at least one wearable garment can be selected from the group consisting of: vest; shirt; bib; arm band; torso band; any patient-attachable assembly capable of maintaining the one or more electrodes in contact with the torso surface or sufficiently close thereto that a monitorable signal is detectable; and/or combinations thereof.

[0063] In various embodiments, the at least one wearable garment can comprise a first wearable garment and a second wearable garment and the multiple electrodes can be coupled to the first wearable garment, and the one or more ultrasound transducers and one or more ultrasound sensors can be coupled to the second wearable garment.

[0064] In some embodiments, calculating distance information can comprise calculating tissue thickness information.

[0065] In some embodiments, the method can include using the dipole densities $d(y)$ to locate an origin of abnormal electrical activity of a heart.

[0066] In some embodiments, the method can include using the dipole densities $d(y)$ to diagnose at least one of: an arrhythmia; ischemia; or compromised myocardial function.

[0067] In some embodiments, the method can include using the dipole densities $d(y)$ to treat at least one of: an arrhythmia; ischemia; or compromised myocardial function.

[0068] In some embodiments, calculating the dipole densities $d(y)$ can include a processor executing a computer program stored in a memory, the computer program embodying an algorithm for generating a table of dipole densities in the memory.

[0069] In some embodiments, at least one ultrasound transducer can comprise at least one ultrasound sensor.

[0070] In accordance with another aspect of the present disclosure, a device for creating a database of dipole densities $d(y)$ at the epicardial surface and endocardial surface of the heart of a patient comprises: an external array of multiple electrodes positioned proximate the patient's torso surface; an internal array of multiple electrodes positioned within a chamber of the heart; a first receiver configured to receive mapping information from the external and internal array of multiple electrodes; a second receiver configured to receive an anatomical depiction of the heart; a dipole density module configured to generate the database of dipole densities $d(y)$ of polygonal shaped projections onto the epicardial surface and endocardial surface, wherein the dipole density module computes the dipole density at all vertices of the polygonal shaped projections, wherein if the dipole density is $d(y)$, the total measured potential $V(x)$ at a location x is the sum over all vertices of $d(y)$ times a matrix $\omega(x,y)$, and wherein: a) x represents a series of locations on the torso surface; and b) $V(x)$ is a measured potential at point x , said measured potential recorded by the multiple electrodes.

[0071] In some embodiments, the dipole density module can be configured to generate the database of dipole densities $d(y)$ using a finite elements method.

[0072] In some embodiments, the polygonal shaped projections can be substantially the same size.

[0073] In some embodiments, the dipole density can be determined by a number of polygonal shaped projections, wherein the number can be determined by the size of an epicardial surface and endocardial surface.

[0074] In some embodiments, the device can further comprise a wearable garment, and the external array of multiple electrodes can be coupled to the wearable garment.

[0075] In some embodiments, the device can further comprise a catheter, and the internal array of multiple electrodes can be coupled to the catheter.

[0076] In some embodiments, the anatomical depiction of the heart can comprise a generic model of a heart.

[0077] In some embodiments, the device can further comprise: one or more external ultrasound transducers positioned proximate the patient's torso surface, the one or more ultrasound transducers being configured to emit waves toward the epicardial surface; and one or more external ultrasound sensors positioned proximate the patient's torso surface, the one or more ultrasound sensors being configured to receive reflections of the waves from the epicardial surface.

[0078] The device can further comprise at least one wearable garment, and the at least one of the multiple external electrodes, one or more external ultrasound transducers, or one or more external ultrasound sensors can be coupled to at least one wearable garment. The anatomical depiction of the epicardial surface of the heart can comprise real-time anatomical imaging from the one or more external ultrasound transducers and the one or more external ultrasound sensors.

[0079] In some embodiments, the device can further comprise: one or more internal ultrasound transducers positioned within a chamber of the heart, the one or more ultrasound transducers being configured to emit waves toward the endocardial surface; and one or more internal ultrasound sensors positioned within a chamber of the heart, the one or more ultrasound sensors being configured to receive reflections of the waves from the endocardial surface. The at least one of the multiple internal electrodes, one or more internal ultrasound transducers, or one or more internal ultrasound sensors can be coupled to a catheter. The anatomical depiction of the endocardial surface of the heart can comprise real-time anatomical imaging from the one or more internal ultrasound transducers and the one or more internal ultrasound sensors.

[0080] In some embodiments, the device can be configured to diagnose at least one of: an arrhythmia; ischemia; or compromised myocardial function.

[0081] In some embodiments, the device can be configured to treat at least one of: an arrhythmia; ischemia; or compromised myocardial function.

[0082] In accordance with another aspect of the present disclosure, a portable system for obtaining mapping information at an epicardial surface of the heart of a patient comprises: a wearable garment proximate the patient's torso; an array of multiple electrodes coupled to the wearable garment proximate the patient's torso surface; and a device configured to receive mapping information from the multiple electrodes.

[0083] In some embodiments, the multiple electrodes can be wired and/or wirelessly connected to the device.

[0084] In some embodiments, the device can include a recording device configured to record the mapping information.

[0085] In some embodiments, the device can include a communication system configured to transmit the mapping information to a remote location.

[0086] In some embodiments, the device can include a computer configured to receive the mapping information from the multiple electrodes and generate a database of dipole densities $d(y)$. The computer can be further configured to transmit the mapping information and/or dipole densities $d(y)$ to a remote location.

[0087] In some embodiments, the device can be coupled to the wearable garment.

[0088] In some embodiments, the portable system can further comprise: one or more ultrasound transducers coupled to the wearable garment, the one or more ultrasound transducers being configured to emit waves toward the epicardial surface; and one or more ultrasound sensors coupled to the wearable garment, the one or more ultrasound sensors being configured to receive reflections of the waves from the epicardial surface; wherein the portable system is configured to receive information from the ultrasound sensors. The portable system can include a recording device coupled to the one or more ultrasound sensors and configured to receive and record sensor data from the one or more ultrasound sensors. The portable system can include a communication system coupled to the one or more ultrasound transducers and one or more ultrasound sensors and configured to transmit the sensor data from the one or more sensors to a remote location. The portable system can include a computer coupled to the one or more ultrasound transducers and one or more ultrasound sensors, and the computer can be configured to receive sensor data from the one or more sensors and to determine distance measurements to the epicardial surface.

[0089] In some embodiments, the portable system can further comprise one or more functional elements, the one or more functional elements comprising one or more elements selected from the group consisting of: a pressure sensor such as a blood pressure sensor; a pH sensor; a glucose sensor; a respiration sensor; a salinity or other sweat level sensor; an EEG sensor such as an EEG sensor placed on the scalp of the patient; an oxygen level sensor such as an oxygen level sensor placed on the finger of the patient; an eye gaze sensor; and/or combinations of these. The one or more functional elements can be coupled to the wearable garment. The portable system can include a recording device operably coupled to the one or more functional elements and configured to receive and record data from the one or more functional elements. The portable system can include a communication system operably coupled to the one or more functional elements and configured to transmit data from the one or more functional elements to a remote location. The portable system can include a computer operably coupled to the one or more functional elements, and the computer can be configured to receive data from the one or more functional elements. The computer can comprise one or more algorithms constructed and arranged, when executed by at least one computer processor, to analyze one or more of: cardiac geometry; cardiac electrical activity; blood pressure; pH; glucose; respiration; sweat level; brain activity; and/or blood oxygen level. The computer can be configured to analyze cardiac electrical activity and at least one physiologic parameter selected from the group consisting of: blood pressure; pH; glucose; respiration; sweat level; brain activity; and/or blood oxygen level.

[0090] In some embodiments, the system can be configured to diagnose at least one of: an arrhythmia; ischemia; or compromised myocardial function.

[0091] In some embodiments, the system can be configured to treat at least one of: an arrhythmia; ischemia; or compromised myocardial function.

[0092] In accordance with another aspect of the present disclosure, a portable system for obtaining information at an epicardial surface of the heart of a patient comprises: a wearable garment positioned proximate the patient's torso surface having array of multiple electrodes, one or more transducers, one or more sensors and/or one or more functional elements coupled to the wearable garment; and a portable device configured to receive information from the electrodes, transducers, sensors and/or functional elements.

[0093] In some embodiments, the wearable garment can be selected from the group consisting of: vest; shirt; bib; arm band; torso band; any patient-attachable assembly capable of maintaining the one or more electrodes, one or more ultrasound transducers, and/or one or more ultrasound sensors in contact with the torso surface, or sufficiently close thereto that a monitorable signal is detectable; and/or combinations thereof.

[0094] In some embodiments, the functional elements can include an element selected from the group consisting of: a pressure sensor such as a blood pressure sensor; a pH sensor; a glucose sensor; a respiration sensor; a salinity or other sweat level sensor; an EEG sensor such as an EEG sensor placed on the scalp of the patient; an oxygen level sensor such as an oxygen level sensor placed on the finger of the patient; an eye gaze sensor; and/or combinations of these. The portable system can include a computer, and the computer can comprise one or more algorithms constructed and arranged to, when executed by at least one computer processor, analyze one or more of: cardiac geometry; cardiac electrical activity; blood pressure; pH; glucose; respiration; sweat level; brain activity; and blood oxygen level. The computer can be configured to analyze cardiac electrical activity and at least one physiologic parameter selected from the group consisting of: blood pressure; pH; glucose; respiration; sweat level; brain activity; and/or blood oxygen level.

[0095] In some embodiments, the wearable garment includes multiple wearable garments, and the array of multiple electrodes, one or more transducers, one or more sensors and/or one or more functional elements can be coupled to one or more of the multiple wearable garments.

[0096] In some embodiments, the portable system includes a computer coupled to the multiple electrodes and the computer can include one or more algorithms constructed and arranged to analyze mapping information from the multiple electrodes and generate the database of dipole densities $d(y)$.

[0097] In some embodiments, the portable system includes a computer coupled to the one or more ultrasound transducers and one or more ultrasound sensors: the one or more ultrasound transducers being configured to emit waves toward the epicardial surface; the one or more ultrasound sensors being configured to receive reflections of the waves from the epicardial surface; and wherein the computer includes one or more algorithms constructed and arranged to receive sensor data from the one or more sensors to determine distance measurements to the epicardial surface.

[0098] In some embodiments, the system can be configured to diagnose at least one of: an arrhythmia; ischemia; or compromised myocardial function.

[0099] In some embodiments, the system can be configured to treat at least one of: an arrhythmia; ischemia; or compromised myocardial function.

BRIEF DESCRIPTION OF THE DRAWINGS

[0100] FIG. 1 illustrates an exemplary embodiment of a mapping system, in accordance with aspects of the present invention.

[0101] FIG. 2 illustrates a computer architecture forming part of the mapping system of FIG. 1, in accordance with aspects of the present invention.

[0102] FIG. 3 illustrates a schematic view for determining a database table of dipole densities $d(y)$, in accordance with aspects of the present invention.

[0103] FIG. 4 illustrates a schematic view for determining a database table of dipole densities $d(y)$ using finite elements, in accordance with aspects of the present invention.

[0104] FIG. 5 illustrates a flow chart of a method for determining a database table of dipole densities, in accordance with aspects of the present invention.

[0105] FIG. 6 is an example embodiment of a method of determining and storing dipole densities, in accordance with aspects of the present invention.

[0106] FIG. 7 illustrates a schematic view combining both external and internal systems for determining dipole densities $d(y)$ using finite elements, in accordance with aspects of the present invention.

[0107] FIG. 8 illustrates an exemplary embodiment of a home usable mapping system capable of recording or communicating with the physician, in accordance with aspects of the present invention.

DETAILED DESCRIPTION

[0108] Various exemplary embodiments will be described more fully hereinafter with reference to the accompanying drawings, in which some exemplary embodiments are shown. The present inventive concept can, however, be embodied in many different forms and should not be construed as limited to the exemplary embodiments set forth herein.

[0109] It will be understood that, although the terms first, second, etc. are used herein to describe various elements, these elements should not be limited by these terms. These terms are used to distinguish one element from another, but not to imply a required sequence of elements. For example, a first element can be termed a second element, and, similarly, a second element can be termed a first element, without departing from the scope of the present invention. As used herein, the term “and/or” includes any and all combinations of one or more of the associated listed items.

[0110] It will be understood that when an element is referred to as being “on” or “attached”, “connected” or “coupled” to another element, it can be directly on or connected or coupled to the other element or intervening elements can be present. In contrast, when an element is referred to as being “directly on” or “directly connected” or “directly coupled” to another element, there are no intervening elements present. Other words used to describe the relationship between elements should be interpreted in a like fashion (e.g., “between” versus “directly between,” “adjacent” versus “directly adjacent,” etc.).

[0111] The terminology used herein is for the purpose of describing particular embodiments only and is not intended to be limiting of the invention. As used herein, the singular forms “a,” “an” and “the” are intended to include the plural forms as well, unless the context clearly indicates otherwise. It will be further understood that the terms “comprises,” “comprising,” “includes” and/or “including,” when used

herein, specify the presence of stated features, steps, operations, elements, and/or components, but do not preclude the presence or addition of one or more other features, steps, operations, elements, components, and/or groups thereof.

[0112] Spatially relative terms, such as “beneath,” “below,” “lower,” “above,” “upper” and the like can be used to describe an element and/or feature’s relationship to another element(s) and/or feature(s) as, for example, illustrated in the figures. It will be understood that the spatially relative terms are intended to encompass different orientations of the device in use and/or operation in addition to the orientation depicted in the figures. For example, if the device in the figures is turned over, elements described as “below” and/or “beneath” other elements or features would then be oriented “above” the other elements or features. The device can be otherwise oriented (e.g., rotated 90 degrees or at other orientations) and the spatially relative descriptors used herein interpreted accordingly.

[0113] Various exemplary embodiments are described herein with reference illustrations of idealized or representative structures and intermediate structures. As such, variations from the shapes of the illustrations as a result, for example, of manufacturing techniques and/or tolerances, are to be expected. Thus, exemplary embodiments should not be construed as limited to the particular shapes of regions illustrated herein but are to include deviations in shapes that result, for example, from manufacturing.

[0114] The catheters and other devices described in accordance with aspects of the present invention can include numerous forms of diagnostic catheters, such as catheters including one or more electrodes, or therapeutic catheters such as tissue ablation catheters. Catheters can be introduced percutaneously into a patient’s heart, such as to record electrical activity, measure distances between structures, or deliver energy. External devices and systems can be included, such as body surface electrodes used to record electrical activity or deliver an electric signal, or visualization devices such as external ultrasound or fluoroscopic imaging systems. Any of these catheters or other devices can include one or more electrodes and/or one or more ultrasound elements (e.g. one or more ultrasound sensors and/or ultrasound transducers). The electrodes and/or ultrasound elements of the present invention can be positioned at any location on the device, for example at a distal or proximal portion of the device, and can be positioned internal or external to a patient’s body.

[0115] Any or all of the ultrasound elements (e.g. ultrasound transducers and/or ultrasound sensors) of the present invention can be used to measure a distance between a sensor and/or a transducer and a surface, as is known in the art. One example includes measuring the distance between an ultrasound element comprising a sensor-transducer pair and a wall of a chamber of the heart.

[0116] Any or all of the electrodes of the present invention can be used to record electric “signals” (e.g. voltages and/or currents) at or between one or more electrode locations. Recorded electric signals can be used to map electrical activity of tissue. The mapped electrical activity can be further processed (e.g. in terms of sources of charge and charge density and correlated with various physiologic parameters related to the function of the heart) and the mapped electrical activity and other recorded and calculated information can be provided visually to one or more operators of the system of the present invention.

[0117] Any or all of the electrodes of the present invention can be used to deliver and/or record electric signals that are generated by the system. Such delivered signals can be emitted from any one or more electrodes, and can be delivered between any two or more electrodes. Recorded signals can comprise a signal present at a single electrode location or at multiple electrode locations (e.g. a signal representing a comparison of two or more signals present at two or more electrode locations). Recorded signals can be measured, for example, synchronously or asynchronously in terms of voltage and/or current. Recorded signals can be further processed in terms of, for example, resistive and reactive components of impedance and/or the combined magnitude of impedance with any original or processed signal “values” (e.g. those represented by a parameter selected from the group consisting of: instantaneous amplitude; phase; peak; Root-Mean-Square (rms); demodulated magnitude; and combinations of these).

[0118] The terms “map” and “mapping” shall include, but need not be limited to, “electrical map”, “electrical mapping”, “anatomical map”, “anatomical mapping”, “device map” and “device mapping”, each of which is defined herein below.

[0119] The terms “electrical map” and “electrical mapping” shall include, but need not be limited to, recording, processing and/or displaying electrical information, such as electrical information recorded by one or more electrodes described or understood in accordance with the present invention. This electrical information includes, but is not limited to: cardiac or other tissue voltage measurements; cardiac or other tissue bipolar and/or unipolar electrograms; cardiac or other tissue surface charge data; cardiac or other tissue dipole density data; cardiac or other tissue monophasic action potentials; and combinations of these.

[0120] The terms “anatomical map” and “anatomical mapping” shall include, but need not be limited to, recording, processing and/or displaying anatomical information, such as anatomical information provided by one or more ultrasound elements of the present invention and/or one or more electrodes described or understood in accordance with the present invention. This anatomical information includes, but is not limited to: two-dimensional (2D) or three-dimensional (3D) representations of tissue, such as one or more chambers of a heart; tissue wall thicknesses such as the thickness of an atrial or ventricular wall; distance between two tissue surfaces; and combinations of these. In some embodiments, a dipole density map and/or surface charge map (hereinafter singly or collectively dipole density map) is provided by using information provided by multiple electrodes and multiple ultrasound elements, such as is described in Applicant’s co-pending international application, Serial Number PCT/US2012/028593, entitled “Device and Method For the Geometric Determination of Electrical Dipole Densities on the Cardiac Wall”, the entirety of which is incorporated herein.

[0121] The terms “device map” and “device mapping” shall include, but need not be limited to, recording, processing and/or displaying of device distance information, such as information comprising the distance between a device or device component and another object, such as tissue or another device or device component.

[0122] Any pair of electrodes described or understood in accordance with the present invention can be constructed and arranged to provide distance information, such as the distance between that pair of electrodes, or the distance between one of the electrodes and one or more proximate components (e.g. a

component at a known distance from one or both of the electrodes in the pair). By delivering and recording an electric signal between electrodes of known separation distances, the signal can be processed and/or calibrated according to one or more known separation distances (e.g. the separation distance between two electrodes fixedly mounted to a rigid structure at a pre-determined distance). Calibrated signal values can be combined across adjacent sets of electrode pairs to accurately estimate the distance between any pair (e.g. any arbitrary pair of electrodes on any one or more devices of the system) of electrodes for which the separation distance is not known. Known and calculated separation distances can be used as “reference” electrodes and combined to triangulate the unknown position of one or more “marker” electrodes, such as an electrode positioned on the present invention or on a separate or external device and positioned proximate the present invention. The process of triangulation can be used to dynamically localize the three-dimensional position of any or all of the electrodes either individually and/or as a combined entity in three-dimensional space.

[0123] Further, any or all electrodes described or understood in accordance with the present invention, such as one or more electrodes placed inside a chamber of a heart, can be used to deliver electric energy, such as radiofrequency energy.

[0124] In accordance with aspects of the present invention, provided is an improved device, system and method for calculating and visualizing the distribution and activity of dipole densities and/or surface charge (hereinafter singly or collectively dipole densities) on the epicardial surface of the heart, and in some embodiments, dipole densities on both the epicardial and endocardial surfaces simultaneously. The dipole densities can be determined by a finite elements method, avoiding the errors encountered using previous extrapolation algorithms.

[0125] Calculating surface charge and/or dipole densities of the heart with internal electrodes has been described in detail in U.S. Pat. No. 8,417,313 (hereinafter the ‘313 patent), entitled “Method and device for determining and presenting surface charge and dipole densities on cardiac walls”.

[0126] As discussed in the ‘313 patent, research indicated that the use of the surface charge densities (i.e. their distribution) or dipole densities (i.e. their distribution) to generate distribution map(s) would lead to more detailed and precise information on electric ionic activity of local cardiac cells than potentials. Surface charge density or dipole densities represent precise information of the electric activity with a compact spatial resolution, whereas potentials resulting from integration of charge densities provide only a diffuse picture of electric activity. The electric nature of cardiac cell membranes comprising ionic charges of proteins and soluble ions can be precisely described by surface charge and dipole densities. The surface charge densities or dipole densities cannot be directly measured in the heart, but instead must be mathematically and accurately calculated starting from measured potentials. In other words, the information of voltage maps obtained by current mapping systems can be greatly refined when calculating surface charge densities or dipole densities from these.

[0127] The surface charge density means surface charge (Coulombs) per unit area (cm^2). A dipole, as such, is a neutral element, wherein a part comprises a positive charge and the other part comprises the same but negative charge. A dipole

can better represent the electric nature of cellular membranes, because in a biological environment ion charges are not macroscopically separated.

[0128] A device for determining dipole densities on the heart wall with internal electrodes has been described in detail in U.S. Patent Publication No. US2010/0298690 (hereinafter the '690 publication) and Patent Cooperation Treaty Publication No. WO2012/122517 (hereinafter the '517 publication), entitled "Device and method for the geometric determination of electrical dipole densities on the cardiac wall.

[0129] The '517 publication disclosed devices, systems, and methods for determining the dipole densities on heart walls using one or more catheters placed into the heart chamber. In particular, a triangularization of the heart wall is performed in which the dipole density at each vertex correlate to the potential measured at various locations within the associated chamber of the heart. To create a database of dipole densities, mapping information recorded by one or more electrodes located on one or more catheters and anatomical information is used. Additionally, one or more ultrasound elements are provided on the catheter.

[0130] While the '313 patent, '690 publication and '517 publication disclose devices, systems, and methods for creating an image of the heart based on information recorded from one or more internal electrodes (e.g. creating an anatomical and/or electrical representation of the heart), some embodiments of the present invention disclose devices, systems, and methods for creating a heart image with external sensors (i.e. external sensors only), while other embodiments disclose devices, systems, and methods using both internal and external sensors to create the heart image.

[0131] For imaging of the heart with external sensors, one or more electrodes outside the body (external) can be positioned proximate the surface of the patient's torso. In some embodiments, one or more ultrasound elements (e.g. one or more ultrasound transducers, sensors or combined transducer-sensors, hereinafter "ultrasound element") can also be used with the one or more electrodes outside the body, such as one or more ultrasound elements also positioned proximate the surface of the patient's torso.

[0132] For the combination of signals from both external and internal sensors to create an image of the heart, the external one or more electrodes disclosed in the present invention are used with internal (inside the body) electrodes disclosed in the internal sensor-based devices, systems, and methods of the '313 patent, '690 publication and '517, combining heart chamber geometry with internal and external sensor (voltage) readings, such that dipole densities can be depicted as an animated color map of activation for each heart beat across the epicardial and/or endocardium surface. The information can be used to diagnose and/or treat a patient with a cardiac arrhythmia, such as atrial fibrillation, or an inadequately synchronized activation sequence, such as in heart failure. Other information obtained can include precise location of foci, conduction-gaps, and/or position of conduction channels.

[0133] In some embodiments of the present invention, a dipole density library can be created in computer memory by combining the electrode voltage readings from one or more electrodes proximate the surface of the patient's torso with anatomical imaging from an imaging instrument, such as CT; MRI; ultrasound; and/or a generic model of a heart. This anatomical imaging can be generated in real-time and/or

imported from previous imaging from one or more of CT, MRI, ultrasound (internal or external), or other imaging apparatus.

[0134] In some embodiments of the present invention, the dipole density library is created by combining the electrode voltage readings from one or more electrodes with ultrasound readings recorded by the one or more ultrasound elements proximate the surface of the patient's torso. Alternatively or additionally, the dipole density library is created by combining the electrode voltage readings from one or more electrodes with ultrasound readings recorded by one or more ultrasound elements positioned within the patient's body, such as one or more ultrasound elements positioned within one or more chambers of the patient's heart.

[0135] In some embodiments, the system of the present invention comprises an external device, for example a vest, having one or more electrodes, and optionally, one or more ultrasound elements. FIG. 1 shows an example embodiment of a mapping system **100** that can be used for real time dipole density mapping of a heart **12** of a human **10**. System **100** can include a computer **110** having known types of input devices and output devices, such as a display **120** and printer **130**, coupled to a patient attachment device, vest **140**, having one or more electrodes **142**. In some embodiments, vest **140** can further include one or more ultrasound elements **144**. Ultrasound elements **144** can include one or more ultrasound transducers configured to transmit ultrasound waves, such as sound waves configured to reflect off of one or more structures of the heart, and be recorded or otherwise received by one or more ultrasound sensors. Alternatively or additionally, ultrasound elements **144** can include one or more ultrasound sensors, such as one or more ultrasound sensors which receive the reflected sound waves. In some embodiments, one or more ultrasound elements **144** can include both an ultrasound transmitter and an ultrasound sensor, such as a single element that both transmits and receives ultrasound waves.

[0136] While a vest is shown, numerous alternative patient attachment device types can be used, including, for example, shirts, bibs, arm bands, torso bands and/or any other patient-attachable assembly capable of maintaining the one or more electrodes **142** and/or ultrasound elements **144** in contact with the wearer's body, or sufficiently close thereto, such that a signal can be detected and/or transmitted by each signal-detecting element. Alternatively or additionally, the one or more electrodes **142** and/or ultrasound elements **144** can be attached directly to the skin. In some embodiments, multiple discrete attachments can be used with a combination of garments, (e.g. shirt plus armband or torso band plus armband), or a combination of a garment with direct skin attachment(s).

[0137] In some embodiments, vest **140** can only include one or more electrodes **142**, with no ultrasound elements. In other embodiments, vest **140** can include one or more ultrasound elements **144**, and not have any electrodes. In still other embodiments a combination of garments can be used with different elements being positioned on different garments. For example, in a combination of shirt plus armband, the shirt can have one or more electrodes **142** while the armband can have one or more ultrasound elements **144**.

[0138] In some embodiments, vest **140** is flexible and conforms closely to the body of the patient and can be made of any suitable materials. Vest **140** can be configured so that the one or more electrodes **142** and/or ultrasound elements **144** are urged against the skin at a consistent position, such as to prevent movement of the element across the skin. In some

embodiments, the one or more electrodes **142** and/or ultrasound elements **144** can be positioned on both the front and the back of the patient. In other embodiments, the one or more electrodes **142** and/or ultrasound elements **144** can be positioned only on the front or back of the patient, depending on application.

[0139] The one or more electrodes **142** and/or ultrasound elements **144** can be connected to computer **110**, such as via a wired and/or wireless connection (see FIG. **8**). Computer **110** can control the operation of the one or more electrodes **142** and/or ultrasound elements **144**. In some embodiments, computer **110** can shut off selected electrodes **142** and/or ultrasound elements **144**, leaving only the associated electrodes **142** and/or ultrasound elements **144** that cover one or more areas of interest being turned on.

[0140] System **100** can be used to create a three-dimensional database of dipole densities $d(y)$ and distance measurements at the epicardial surface of the heart. The distance measurements can include, but are not limited to: the distance between at least one of the electrodes **142** and the epicardial surface, the distance between at least one of the electrodes **142** and an ultrasound element **144**, and the distance between the epicardial surface and an ultrasound element **144**. Knowing the speed of sound in the particular environment, as well as the timing of the delivery of sound waves by the transducer, the distance between an ultrasound transducer, a reflected surface, and an ultrasound sensor can be calculated, as described herein below. Alternatively or additionally, the distance measurements can be calculated by analyzing the received signal amplitude, a shift in frequency between transmitted and received signals, and/or an ultrasound sensor recorded angle. System **100** can also be configured to produce continuous, real time geometries of the tissue of a patient. System **100** can provide one or more of: tissue geometry information such as tissue position, tissue thickness (e.g. cardiac wall thickness) and tissue motion (e.g. cardiac wall motion) information; distance information such as distance between two tissue locations, and distance between a tissue location and a device component location; tissue electrical activity information; status of ablation of a portion of tissue; status of resynchronization pacing, and/or combinations of these.

[0141] In some embodiments, the present invention incorporates one or more ultrasound elements **144** comprising both an ultrasound transducer and an ultrasound sensor, each preferably contained in a single component. The ultrasound sensor is configured to record or otherwise detect the wave reflections that result from the ultrasound waves emitted from one or more ultrasound transducers. In addition to determining real-time continuous anatomical geometry information, the detected wave reflections can be used to determine real-time continuous measurements of the position of at least one of the electrodes **142** and/or at least one ultrasound element **144**. This information can be used to enhance one or more dipole density $d(y)$ calculations. Measurements can be taken to determine the thickness of an object, such as the thickness of cardiac tissue, which can be used to determine an ablation parameter such as power or time of energy delivery.

[0142] In a typical embodiment, an ultrasound element **144** comprising a piezo crystal transmits acoustic waves and receives the reflections of those waves. As is well known to those skilled in the art, the timing between transmitting and receiving can be used to determine the distance between the transmitting and receiving surfaces, and one or more reflec-

tive surfaces (e.g. reflective tissue surfaces). In some embodiments, precise distances and dimensions of target cardiac tissue is determined, resulting in a more precise and effective diagnosis and/or therapy.

[0143] By having precise anatomical and other distance information, the dipole density calculations will be similarly precise. In some embodiments, one or more ultrasound elements **144** are constructed and arranged to produce sound waves in at least one of either constant or pulsed excitation, such as sound waves between 3 megahertz and 18 megahertz. The waves emitted by one or more ultrasound elements **144** can be at constant frequency and/or produced by a chirp of changing frequency (to allow pulse compression or demodulation on reception). The precision in dipole density calculations along with the distance measurements will allow for the precise detailing of the electrical activity in the cardiac cells and will allow for the precise identification of which cells are the earliest sites of activation. In some embodiments, one or more ultrasound elements **144** can be configured to automatically detect the distance from one or more ultrasound elements **144** to the epicardial surface via a first reflection and further detect the cardiac wall thickness via a second reflection. In another embodiment, one or more ultrasound elements **144** integrate multiple reflections to construct an anatomical geometry including an epicardial surface of the heart and the thickness of the associated myocardium.

[0144] In some embodiments, one or more ultrasound elements **144** include at least one crystal, typically comprised of a piezoelectric material, which is positioned proximate to the center of each electrode **142** within an electrode array. In another embodiment, one or more ultrasound elements **144** include at least one crystal positioned between two or more electrodes **142**, such as to create a device with a ratio of mapping electrodes **142** to ultrasound elements **144** of 1:1, 2:1, 5:2, 3:1, 4:1 or another ratio. The at least one crystal can be constructed and arranged to transmit ultrasonic signals and/or to receive ultrasonic signals (e.g. receive ultrasonic signals transmitted by the same or different crystals and/or the reflections of those signals). In another embodiment, one or more ultrasound elements **144** comprise a plurality of crystals, such as a plurality of crystals arranged in an array.

[0145] In some embodiments, one or more ultrasound elements **144** comprise a piezoelectric film covering one or more electrodes **142**, such as one or more electrodes **142** within an array. In some embodiments, one or more ultrasound elements **144** can be constructed as part of an electrode **142**. For example, system **100** can comprise a sensor/electrode combination.

[0146] FIG. **2** provides an example embodiment of a computer architecture **200** that can form part of mapping system **100**. Architecture **200** includes interface module **210** for interfacing with the vest **140**, interface module **220** for interfacing with output devices **120**, **130**, and at least one processor **240**. The computer **110** includes at least one computer memory **250**. The foregoing are generally known, however the present invention further includes an electric-potential to surface-charge-density and/or dipole-density converter module **230**. Converter module **230** includes instructions necessary for carrying out the methods described herein, when executed by processor **240**, wherein the results of such processing are stored in memory **250**, as would be understood by one skilled in the art having the benefit of this disclosure.

[0147] In some embodiments, the 3D geometry can be accommodated by integrating anatomical data from CT/MRI

scans with the epicardial geometry determined from analysis of the received acoustic signals. The CT/MRI scans can include data to determine torso geometry. The CT/MRI scans can also provide data associated with an epicardial surface surrounding the heart, where those of ordinary skill would understand that the epicardial surface can be used to register the CT/MRI data with data calculated from the devices of the present invention. Further, locating the epicardial surface can include determining or otherwise providing data to be associated with the location of the heart within the torso.

[0148] In accordance with some embodiments of the invention, system 100 is configured to generate a table of dipole densities $v(P, t)$ that embody an ionic nature of cellular membranes across the epicardium of a given heart of a patient, comprising:

[0149] a) a measuring and recording unit that measures and records electric potential data V_e at given positions P proximate the patient's torso surface,

[0150] b) an a/d-converter that converts the at least one electric potentials V_e into digital voltage data,

[0151] c) a processor that transforms the digital voltage data into dipole charge density data, and

[0152] d) a memory that stores the electric potential data V_e and the transformed cellular membrane dipole density data.

[0153] Referring again to FIG. 2, architecture 200 includes a measuring and recording unit, such as interface module 210 which is configured to obtain electric potential data V_e at given positions P proximate the patient's torso surface, the converter module 230 includes an a/d-converter that converts the electric potentials V_e into digital voltage data, the processor 240 transforms the digital voltage data into dipole charge density data, and the memory 250 stores the electric potential data V_e and the transformed cellular membrane dipole density data.

[0154] The measuring and recording unit includes multiple electrodes positioned proximate the patient's torso surface. In some embodiments, the system can further include a wearable garment and at least one of the multiple electrodes can be coupled to the wearable garment. In some embodiments, the wearable garment is flexible and conforms closely to the patient's torso surface and can urge one or more electrodes against the torso surface with a consistent position to prevent movement of the one or more electrodes. The wearable garment can be selected from the group consisting of: vest; shirt; bib; arm band; torso band; any patient-attachable assembly capable of maintaining the one or more electrodes in contact with the torso surface or sufficiently close thereto; and/or combinations thereof.

[0155] In some embodiments, the processor includes a computer program embodying an algorithm that, when executed, transforms the digital voltage data into cellular membrane dipole density data.

[0156] In some embodiments, the system further includes one or more ultrasound transducers positioned proximate the patient's torso surface, the one or more ultrasound transducers being configured to emit waves toward an epicardial surface, and one or more ultrasound sensors positioned proximate the patient's torso surface, the one or more ultrasound sensors being configured to receive reflections of the waves from the epicardial surface, wherein the measuring and recording unit further measures and records the sensor information. In some embodiments, one or more ultrasound transducers are further configured to function as an ultrasound sensor.

[0157] In some embodiments, the processor is configured to receive sensor data from the one or more sensors and generate distance measurements from the epicardial surface. The distance measurement can be produced by analyzing at least one of: timing of received signal; recorded signal amplitude; sensor recorded angle; or signal frequency changes

[0158] In some embodiments, the system includes more than one wearable garment and the multiple electrodes, ultrasound transducers, or ultrasound sensors are coupled to different wearable garments. For example, the multiple electrodes are coupled to a first wearable garment, and the ultrasound transducers and ultrasound sensors are coupled to a second wearable garment. The wearable garments can be selected from the group consisting of: vest; shirt; bib; arm band; torso band; any patient-attachable assembly capable of maintaining the one or more electrodes, one or more ultrasound transducers, and one or more ultrasound sensors in contact with the torso surface, or sufficiently close thereto that a monitorable signal is detectable.

[0159] In some embodiments, the system further includes an imaging unit that represents the cellular membrane dipole densities $v(P, t)$ as a two-dimensional image or time-dependent sequence of images

[0160] In some embodiments, the system further includes an imaging unit that represents the cellular membrane dipole densities $v(P, t)$ as a three-dimensional image or time-dependent sequence of images.

[0161] FIG. 3 shows a schematic view of some elements of computer 110 used for determining a database table of dipole densities $d(y)$. Computer 110 includes a first receiver 310 configured to receive electrical potentials from the one or more electrodes, such as electrodes 142 of FIG. 1. Computer 110 further includes a second receiver 320 configured to receive cardiac geometry information from an imaging instrument, such as CT; MRI; ultrasound; or a generic model of a heart. This anatomical imaging can be generated in real-time and/or imported from previous imaging from one or more of CT, MRI, ultrasound (internal or external), or other imaging apparatus. Dipole density processor 330 receives electrical information from first receiver 310 and cardiac geometry information from the second receiver 320. Dipole density processor 330, which can comprise converter module 230 and processor 240, includes a mathematical processing element or other electronic module including software and/or hardware for performing mathematical or other calculations. Dipole density processor 330 preferably uses one or more algorithms to process the received electrical and geometry information to produce a database table of dipole densities $d(y)$ 350. Alternatively or additionally, dipole density processor 330 can be configured to produce a database table of surface charge information.

[0162] As discussed above, in some embodiments the vest 140 can further include one or more ultrasound transducers and/or one or more ultrasound sensors to provide cardiac geometry information to the second receiver 320. The one or more ultrasound transducers transmit ultrasound waves, such as waves configured to reflect off one or more structures of the heart, and be recorded by the ultrasound sensors (e.g. reflections from the epicardial surface and one or more of the inner surfaces or structures of the heart). Dipole density processor 330 receives electrical information from first receiver 310 and ultrasound cardiac geometry information from the second receiver 320. Dipole density processor 330, which can comprise converter module 230 and processor 240, includes a

mathematical processing element or other electronic module including software and/or hardware for performing mathematical or other calculations. Dipole density processor 330 preferably uses one or more algorithms to process the received electrical and geometry information to produce a database table of dipole densities $d(y)$ 350.

[0163] The geometric model of the epicardial surface can be processed by the dipole density processor 330 into multiple small triangles (triangularization) and/or other polygonal shapes (e.g., squares, tetrahedral, hexagonal, and others). When the polygons are sufficiently small, the dipole density has a small variation over the polygon. In a preferred embodiment, the number of triangles is determined by dipole density processor 330. With the electrodes positioned by a clinician, such as an electrophysiologist, the potentials at each electrode are recorded. The dipole density processor 330 computes the dipole density at all vertices of the triangles. If the dipole density at a vertex is $d(y)$, the total measured potential $V(x)$ at a location x is the sum over all vertices y of $d(y)$ times a matrix $W(x,y)$. A detailed description is provided in reference to FIG. 4.

[0164] In a preferred embodiment, dipole density processor 330 implements a progressive algorithm that can be modified and/or refined in order to improve spatial and/or time resolution of the database of dipole densities that are produced. The dipole densities $d(y)$ can be obtained by solving a linear system of equations. Thereby a map of dipole densities can be created at each corresponding time interval. The synthesis of the maps generates a cascade of the activation sequence of each corresponding heart beat that can be used to diagnose cardiac wall tissue, such as to identify an origin of aberrant electrical activity or otherwise diagnose an arrhythmia. These sequential activation maps of dipole densities and/or other dipole density information as described herein can be used to diagnose and/or treat numerous forms of cardiac disease such as when the dipole density information is used to diagnose and/or treat an arrhythmia, ischemia and/or compromised myocardial function.

[0165] The measuring electrodes used in the present invention are placed on or proximate the torso surface. Due to the inhomogeneous structure of the body, it is difficult to localize the actual sources of the skin electrode measured potentials. A highly complicated boundary value problem must be solved with boundary conditions that are poorly known. Prior art attempts at determining the "action potential" from body surface ECG (alone) have not been very successful.

[0166] Utilizing the formulas in the '313 patent, '690 publication and '517 publication, the present invention calculates the dipole densities using external electrodes on the vest, in combination with cardiac geometry information from an imaging instrument (such as CT; MRI; ultrasound); or the optional external ultrasound transducers and/or ultrasound sensors on the vest.

[0167] Referring now to FIG. 4, an embodiment of a system for determining a database table of dipole densities $d(y)$ of a patient is illustrated. System 100, shown in FIG. 1, is configured to create a database table of three-dimensional dipole densities $d(y)$ based on voltage potentials and image information relating to the heart, as has been described above.

[0168] As shown in FIG. 4, triangle T1, defined by system 100 is at location Y1. The contribution of triangle T1 to the potential at location X1 can be computed from the dipole density at the vertices of T1. The dipole density processor 330 determines the desired dipole density $d(y)$ from the total

measured potential $V(x)$, which is the sum resulting from all the triangles defined by system 100.

[0169] When sufficient potential values $V(x)$ are measured (e.g. from 10 to 10,000 with increasing number of measured potentials providing more accurate results), the dipole density $d(y)$ at many equally distributed vertices y on the epicardial surface is calculated (e.g. from 10 to 50,000 with increasing number of calculated potentials providing more detailed results) by solving a system of linear equations. By interpolation of the measured and/or calculated potentials (e.g. with application of splines) their number can be increased to a higher number of regions. This calculation of dipole density results, such as via an automatic computer program forming at least part of dipole density processor 330.

[0170] In some embodiments, the results are presented in a visual, anatomical format, such as depicting the dipole densities on a geometric model of the epicardial surface in relation to time (t). This format allows a clinician, such as an electrophysiologist, to determine the activation sequence, or other electrical and mechanical measures, on the epicardial surface, such as to determine treatment locations for a cardiac arrhythmia or other inadequacy in cardiac tissue health, such as force of tissue contraction and motion of the epicardial surface. The results can be shown on a display unit 120, or on a separate display not shown, such as a color display. In some embodiments, the device of the present invention is implemented as, or includes, a software program that is executable by at least one processor. The software program can be integrated into one or more of: an ECG system; a cardiac tissue ablation system; an imaging system; a computer; and combinations of these.

[0171] FIG. 5 illustrates one embodiment of a method for determining a database table of dipole densities $d(y)$ of the epicardial surface of a patient's heart. In Step 10, a vest having an array of one or more electrodes (e.g. vest 140 of system 100 of FIG. 1) is placed on the torso of the patient. In Step 20, the geometry of the epicardial surface can be obtained in relation to the positions of the one or more electrodes disposed within the electrode array. In addition to the epicardial surface geometry, the magnitude and other properties of motion of cardiac wall tissue can be determined. In addition, the thickness of a patient's heart tissue can be determined. This information will enable a clinician to determine what treatment, (e.g., what ablation parameters) can be appropriate for the patient. One or more ultrasound transducers and sensors can be utilized in this step, as discussed above. Alternatively or additionally, the geometry of the epicardial surface is obtained in relation to the electrode array position, such as by importing a geometry model from an imaging study (e.g., using computed tomography, MRI and/or ultrasound). The surface of the geometry of the corresponding epicardial surface is generally divided into small polygons, such as in the form of at least 1000 triangles of similar size.

[0172] In Step 30, the dipole density $d(y)$ can be calculated at each vertex y from the measured potential values x . The measurements can be repeated successively during the cardiac cycle, such as once each millisecond, giving the electrophysiologist a dynamic progression of the activation sequence. The information of the time dependent dipole densities can be depicted as an animated color map of activation for each heart beat across the epicardial surface. The information can be used to diagnose and/or treat a patient with a cardiac arrhythmia, such as atrial fibrillation, or an inadequately synchronized activation sequence, such as in heart

failure. Other information obtained can include precise location of foci, conduction-gaps, and/or position of conduction channels.

[0173] The dipole density information can be used to determine cardiac tissue treatment locations for lesion creation, such as a lesion created by a catheter-based ablation system. Alternatively, the lesion can be created by an RF, ultrasound, microwave, laser and/or cryogenic energy ablation catheter. The information can also be used to determine the location of pacing electrodes for cardiac resynchronization therapy.

[0174] In some embodiments, ablating the cardiac tissue can be based upon the tissue diagnosis. For example, the anatomical information comprising tissue thickness information and at least one of the magnitude of ablation energy or the time period in which ablation energy is delivered, is adjusted based on the tissue thickness information recorded by one or more ultrasound sensors.

[0175] FIG. 6 summarizes one method 400 for determining and storing surface charge densities and/or dipole densities in accordance with aspects of the present invention, which have been described in detail above.

[0176] In Step 402, mapping system 100 is used to measure and/or calculate one or more electric potential(s) V_e in one or more position(s) P at a given time t. In Step 404, V_e is transformed into a surface charge density $\rho(P,t)$ and/or dipole density $d(P,t)$. In Step 406, the surface charge density $\rho(P,t)$ and/or dipole density $d(P,t)$ is stored in a database table. The method is repeated if there is another P, in Step 408.

[0177] FIG. 7 shows an embodiment using both external sensor systems and internal sensor systems together. For example, the present systems and methods disclosed above for external sensor-based imaging of the heart can be combined with the devices, systems, and methods using internal sensor-based imaging of the heart disclosed in the '313 patent, '690 publication and '517 publication. FIG. 7 shows the present vest system in combination with system 500, described in detail in the '690 publication and '517 publication, each of which is hereby incorporated by reference. This combination of internal and external electrodes can be used to augment accuracy, specificity, etc., and combining heart chamber geometry with internal and external sensor (voltage) readings can provide simultaneous maps of the epicardium and endocardium walls.

[0178] System 500 includes a mapping catheter with a shaft 311, which is inserted into a chamber of a patient's heart, such as the Left Atrium (LA). At the distal end of shaft 311 is an electrode array 315 including multiple electrodes 316. Electrode array 315 is shown in a basket construction, but numerous other constructions can be used including multiple independent arms, spiral arrays, electrode covered balloons, and other constructions configured to place multiple electrodes into a three-dimensional space. Any catheter with one or more electrodes can be used to supply mapping information to system 100, which is configured to create a database table of three-dimensional dipole densities $d(y)$ based on voltage potentials and image information relating to the heart, as has been described above.

[0179] As shown in FIG. 7, triangle T2, is at location Y2 on the endocardial surface and electrode 316a is at location X2. The contribution of triangle T2 to the potential at location X2 can be computed from the dipole density at the vertices of T1. The dipole density processor 330 determines the desired

dipole density $d(y)$ from the total measured potential $V(x)$, which is the sum resulting from all the triangles defined by system 100.

[0180] When sufficient potential values $V(x)$ are measured (e.g. from 10 to 50,000) with increasing number of measured potentials providing more accurate results, the dipole density $d(y)$ at many equally distributed vertices y on the endocardial surface can be calculated (e.g. from 10 to 50,000 with increasing number of calculated potentials providing more detailed results) by solving a system of linear equations. By interpolation of the measured and/or calculated potentials (e.g. with application of splines) their number can be increased to a higher number of regions.

[0181] In some embodiments, the results are presented in a visual, anatomical format, such as on a display depicting the dipole densities on a geometric model of the endocardial surface and epicardial surface in relation to time (t). This format allows a clinician, such as an electrophysiologist, to determine the activation sequence, or other electrical and mechanical measures, on the endocardial surface and/or epicardial surface, such as to determine treatment locations for a cardiac arrhythmia or other inadequacy in cardiac tissue health, such as force of tissue contraction and motion of an endocardial surface and/or an epicardial surface. The results can be shown on a display unit 120, or on a separate display not shown, such as a color display.

[0182] FIG. 8 shows embodiments for a mapping system 600 for monitoring of a patient at their home or otherwise remote from a clinical setting. The system 600 can use many of the elements and methods described above for determination of dipole densities. The system 600 includes a vest 640, which can use the same or similar features as vest 140 described above, and a recording device 604a, computer 604b and/or communication system 604c.

[0183] Vest 640 can include one or more electrodes 642. In some embodiments, vest 640 can further include one or more ultrasound elements 644, such as one or more ultrasound transducers and/or ultrasound sensors. Vest 640 can be flexible and conform closely to the body of the patient and can be made of any suitable materials. Vest 640 can be configured so that the one or more electrodes 642 and/or ultrasound elements 644 are urged against the torso surface or skin at a consistent position, such as to prevent movement of the element across the skin. In some embodiments, the one or more electrodes 642 and/or ultrasound elements 644 can be positioned on both the front and the back of the patient. In other embodiments, the one or more electrodes 642 and/or ultrasound elements 644 can be positioned on only the front or back of the patient, depending on application. Alternatively, the one or more electrodes 642 and/or ultrasound elements 644 can be attached directly to the skin. While the description discloses one or more electrodes 642 and/or one or more ultrasound elements 644 used with the vest, garment, or direct skin attachment, the invention also envisions embodiments that only include electrodes 642 or only ultrasound elements 644.

[0184] In some embodiments, vest 640 or another component of system 600 includes one or more additional sensors or transducers, functional element 645. Functional elements 645 can comprise an element selected from the group consisting of: a pressure sensor such as a blood pressure sensor; a pH sensor; a glucose sensor; a respiration sensor; a salinity or other sweat level sensor; an EEG sensor such as an EEG sensor placed on the scalp of the patient; an oxygen level

sensor such as an oxygen level sensor placed on the finger of the patient; an eye gaze sensor; and combinations of these.

[0185] The one or more electrodes 642, ultrasound elements 644, and/or functional elements 645 can be coupled to the recording device 604a, computer 604b and/or communication system 604c, with either a wired (not shown) or wireless connection (e.g., Bluetooth, Wi-Fi, or other wireless means). The recording device 604a, computer 604b and/or communication system 604c can control the operation of the one or more electrodes 642, ultrasound elements 644, and/or functional elements 645. This control feature can be programmed into their systems or can be done remotely via a remote connection (e.g., from a physician's office 608). In some embodiments, the recording device 604a, computer 604b and/or communication system 604c can turn on or shut off selected electrodes 642, ultrasound elements 644, and/or functional elements 645, leaving only the associated electrodes 642, ultrasound elements 644, and/or functional elements 645 that cover one or more areas of interest being turned on.

[0186] In some embodiments, the recording device 604a can be a portable device for monitoring and recording various electrical and/or other signal activities of the one or more electrodes 642, ultrasound elements 644, and/or functional elements 645, similar to a Holter or other mobile-patient monitor. The recording device 604a can be configured to continuously monitor and record, or only record on an as needed basis when a recordable event happens. Once the data is recorded, the recording device 604a can be transmitted to the physician's office to be analyzed. In other embodiments, the recording device 604a can be a smart phone, such as a Galaxy S4, having an application for recording the signal activities. Once recorded, the smart phone can also be capable of transmitting the information, for example, to the physician's office.

[0187] In some embodiments, the computer 604b can have the capability of continuously monitoring various signal activities of the one or more electrodes 642, ultrasound elements 644, and/or functional elements 645. The computer 604b can also have the capability of analyzing the data from the one or more electrodes 642, ultrasound elements 644, and/or functional elements 645, similar to system 100 described above. In some embodiments, computer 604b comprises one or more algorithms constructed and arranged to analyze one or more of: cardiac geometry; cardiac electrical activity; blood pressure; pH; glucose; respiration; sweat level; brain activity; or blood oxygen level. In some embodiments, computer 604b analyzes cardiac electrical activity and at least one physiologic parameter selected from the group consisting of: blood pressure; pH; glucose; respiration; sweat level; brain activity; or blood oxygen level. The computer 604b can save the monitored or analyzed data in memory, such as on memory card or flash device card or copy it to a disk. The computer 604b can further have the capability of transmitting the analyzed data, for example, to the physician's office, giving the physician real-time feedback as to the health and condition of their patient.

[0188] In some embodiments, communication system 604c can include a means of communicating with the physician's office on a real-time basis for remote medical patient monitoring, such as over the internet or other direct communica-

tion means (e.g., smart phone). In this way, the physician can monitor the patient 24 hours a day and/or at any time. The system can further include two way communications such that the physician can view the data in real-time while speaking with the patient. The physician can also turn on or shut off selected electrodes 642, ultrasound elements 644 and/or functional elements 645, leaving only the associated electrodes 642, ultrasound elements 644 and/or functional elements 645 that cover one or more areas of interest being turned on.

[0189] Other embodiments of the invention will be apparent to those skilled in the art from consideration of the specification and practice of the embodiments disclosed herein. It is intended that the specification and examples be considered as exemplary only, with a true scope and spirit of the invention being indicated by the following claims. In addition, where this application has listed the steps of a method or procedure in a specific order, it can be possible, or even expedient in certain circumstances, to change the order in which some steps are performed, and it is intended that the particular steps of the method or procedure claims set forth herein below not be construed as being order-specific unless such order specificity is expressly stated in the claim.

1. A device that generates a table of dipole densities $v(P,t)$ that embody an ionic nature of cellular membranes across the epicardium of a given heart of a patient, comprising:

- a) a measuring and recording unit that measures and records electric potential data V_e at given positions P proximate the patient's torso surface;
- b) an a/d-converter that converts the electric potential data V_e into digital voltage data;
- c) a processor that transforms the digital voltage data into cellular membrane dipole density data; and
- d) a memory that stores the electric potential data V_e and the transformed cellular membrane dipole density data.

2.-33. (canceled)

34. A method of creating a database of dipole densities $d(y)$ at the epicardial surface of the heart of a patient, the method comprising:

- placing an array of multiple electrodes proximate the patient's torso surface; and
- calculating dipole densities $d(y)$ by:
 - receiving mapping information from the multiple electrodes;
 - receiving an anatomical depiction of the heart; and
 - generating the database of dipole densities $d(y)$ with a dipole density module, wherein the dipole density module determines dipole densities $d(y)$ of polygonal shaped projections onto the epicardial surface, wherein the dipole density module computes the dipole density at all vertices of the polygonal shaped projections, wherein if the dipole density is $d(y)$, the total measured potential $V(x)$ at a location x is the sum over all vertices of $d(y)$ times a matrix $\omega(x,y)$, and wherein:
 - a) x represents a series of locations on the torso surface; and
 - b) $V(x)$ is a measured potential at point x , said measured potential recorded by the multiple electrodes.

35.-132. (canceled)

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专利名称(译)	用于确定心脏表面上的电偶极子密度的装置和方法		
公开(公告)号	US20160192902A1	公开(公告)日	2016-07-07
申请号	US14/916056	申请日	2014-09-10
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IPC分类号	A61B8/00 A61B5/00 A61B8/08 A61B5/0452 A61B6/03 A61B8/12 A61B18/18 A61B18/02 A61B18/20 A61B5/042 A61B5/0205 A61B3/113 A61B5/044 A61B5/0478 A61B5/04 A61B18/14 A61B5/0432		
CPC分类号	A61B8/4416 A61B2018/00994 A61B5/6805 A61B8/0883 A61B5/0452 A61B6/032 A61B8/12 A61B5 /4836 A61B18/1815 A61B18/02 A61B18/20 A61B5/0422 A61B8/565 A61B5/0205 A61B3/113 A61B5 /044 A61B5/0478 A61B5/04012 A61B8/464 A61B18/1492 A61B5/0432 A61B5/04085 A61B5/1072 A61B2562/046 A61B2576/023 G16H30/40 A61B5/0036		
优先权	61/877617 2013-09-13 US		
外部链接	Espacenet USPTO		

摘要(译)

公开了使用定位在患者躯干上的电极来确定心脏表面上的偶极密度的装置，系统和方法。电极被集成到患者佩戴的一件衣服中。衣服用于固定邻近患者躯干的电极位置。超声换能器和传感器用于确定心外膜表面和电极之间的距离，并且还用于检测心外膜表面运动以及心外膜壁厚度。

